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(54) **ULTRASOUND APPARATUS WITH IMPROVED HEAT DISSIPATION AND METHODS FOR PROVIDING SAME**

5,721,463 A 2/1998 Snyder
5,767,810 A 6/1998 Hagiwara et al.
5,884,693 A 3/1999 Austin et al.

(Continued)

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FOREIGN PATENT DOCUMENTS

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CN 205684415 U * 11/2016
JP 2006130163 A * 5/2006

(Continued)

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OTHER PUBLICATIONS

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 172 days.

Chiang, Alice, PC-Based Ultrasound Imaging System in a Probe, 2000 IEEE Ultrasonics Symposium. Proceedings. An International Symposium (Cat. No. 00CH37121) Date of Conference: Oct. 22-25, 2000, Date Added to IEEE Xplore: Aug. 6, 2002.*

(Continued)

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(57) **ABSTRACT**

(52) **U.S. Cl.**
CPC **A61B 8/546** (2013.01); **A61B 8/4209** (2013.01); **A61B 8/4444** (2013.01); **A61B 8/4472** (2013.01); **A61B 8/4494** (2013.01); **A61B 2562/12** (2013.01)

The present embodiments relate generally to ultrasound apparatus with improved heat dissipation and methods for providing same. The ultrasound apparatus may have a housing that encloses a transducer array and at least one integrated circuit (IC) for driving the transducer array during operation. The housing may have an interior surface and an exterior surface, and the housing can be made substantially of metal. A post is disposed between the at least one IC and the interior surface of the housing. The post can be coupled directly to the interior surface of the housing so that heat generated from the at least one IC is transferred via the post to the housing and dissipated via the exterior surface.

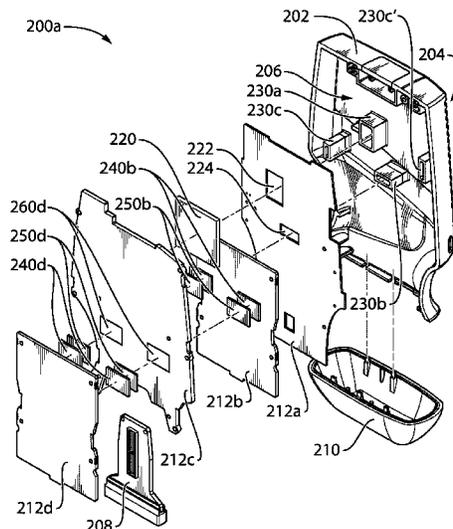
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(56) **References Cited**

U.S. PATENT DOCUMENTS

5,213,103 A 5/1993 Martin et al.
5,560,362 A 10/1996 Sliwa, Jr. et al.

22 Claims, 14 Drawing Sheets



(56)

References Cited

U.S. PATENT DOCUMENTS

5,961,465 A 10/1999 Kelly, Jr. et al.
 6,198,642 B1* 3/2001 Kociecki H02M 1/4225
 307/150
 6,542,846 B1 4/2003 Miller et al.
 6,610,011 B2 8/2003 Emery
 6,905,466 B2 6/2005 Salgo et al.
 7,298,067 B1 11/2007 Kosinski
 7,400,079 B2 7/2008 Omura et al.
 8,054,231 B2 11/2011 Ahn et al.
 8,475,375 B2 7/2013 Smith et al.
 8,695,429 B2 4/2014 Urbano et al.
 8,748,321 B2 6/2014 deVilliers et al.
 8,784,321 B2 7/2014 Courtney et al.
 9,197,011 B2 11/2015 McCormack
 2004/0215079 A1 10/2004 Omura et al.
 2005/0075573 A1 4/2005 Park et al.
 2005/0122271 A1* 6/2005 Pecora, Jr. H01Q 1/40
 343/719
 2005/0129928 A1* 6/2005 Lee B82Y 30/00
 428/323
 2005/0215892 A1 9/2005 Emery et al.
 2006/0139880 A1* 6/2006 Tate G06F 1/20
 361/697
 2006/0173344 A1 8/2006 Marian et al.
 2007/0071266 A1* 3/2007 Little A61B 8/00
 381/328
 2008/0114252 A1 5/2008 Randall et al.
 2008/0188755 A1* 8/2008 Hart A61B 8/00
 600/459
 2008/0194964 A1* 8/2008 Randall A61B 8/00
 600/459
 2008/0214938 A1 9/2008 Solomon et al.
 2009/0043203 A1 2/2009 Pelissier et al.
 2009/0153409 A1 6/2009 Chiang et al.
 2010/0160785 A1* 6/2010 Poland A61B 8/00
 600/459
 2010/0201226 A1 8/2010 Boström
 2010/0228162 A1 9/2010 Sliwa et al.
 2010/0321253 A1 12/2010 Ayala Vazquez et al.
 2011/0018395 A1 1/2011 Ruffa
 2011/0050508 A1 3/2011 Guterman et al.
 2011/0230794 A1 9/2011 van Groningen et al.
 2012/0071710 A1 3/2012 Gazdzinski
 2012/0150038 A1* 6/2012 Osawa G01S 7/5208
 600/443
 2012/0240769 A1 9/2012 Gerner et al.
 2013/0286593 A1 10/2013 Cho et al.

2014/0058270 A1* 2/2014 Davidsen A61B 8/546
 600/472
 2014/0092559 A1* 4/2014 Yamaguchi H05K 7/20336
 361/700
 2014/0111388 A1 4/2014 Di Nallo et al.
 2015/0102965 A1 4/2015 Irci et al.
 2015/0182200 A1 7/2015 Birglehner et al.
 2015/0253290 A1 9/2015 Fujii et al.
 2015/0303551 A1 10/2015 Su et al.
 2015/0351727 A1 12/2015 Nieminen et al.
 2016/0077059 A1 3/2016 Chung et al.
 2018/0031196 A1* 2/2018 Cripps F21S 41/62

FOREIGN PATENT DOCUMENTS

WO 2012156886 A1 11/2012
 WO 2014080312 A1 5/2014
 WO 2015102673 A1 7/2015

OTHER PUBLICATIONS

AMD Global Telemedicine, Trans-Vaginal Ultrasound Probe, Mar. 28, 2016, https://web.archive.org/web/20160328221527/https://www.amdtelemedicine.com/telemedicine-equipment/PDF/AMD_XXX_TransvaginalProbe_lowres.pdf.
 MatWeb Material Property Data, Overview of materials for 7000 Series Aluminum Alloy, <http://www.matweb.com/search/DataSheet.aspx?MatGUID=ab9706916818406b80c22b7f39db0c78&ckck=1>.
 Machine Translation of JP2006130163 (Year: 2006).
 Monteiro, The Influence of Alloy Element on Magnesium for Electronic Devices Applications—A Review, Jun. 11, 2014, DOI: 10.5772/58460, <https://www.intechopen.com/books/light-metal-alloys-applications/the-influence-of-alloy-element-on-magnesium-for-electronic-devices-applications-a-re> (Year: 2014).
 Naumann, H. (2010). “Cellular antenna working inside all-metal case”, available at <http://www.gsm-modem.de/M2M/m2m-faq/cellular-antenna-working-inside-all-metal-case/>, last accessed Mar. 2, 2017.
 Abstract of Hsiao, F (2014). “Dual-band slot antenna suitable for ultrabook application with metal housing”, published in 2014 International Symposium on Antennas and Propagation (ISAP): 317-318. Date of Conference: Dec. 2-5, 2014.
 International Search Report and Written Opinion of the International Searching Authority for Corresponding PCT International Application No. PCT/CA2017/051068 filed Sep. 11, 2017.

* cited by examiner

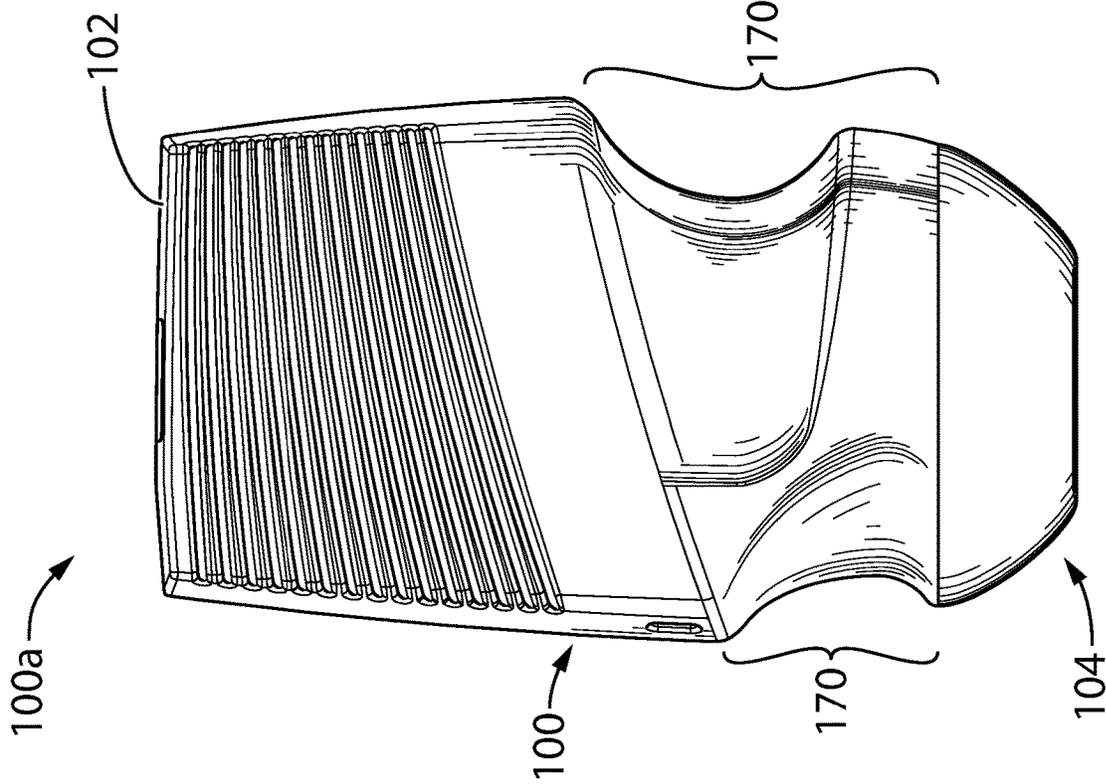


FIG. 1A

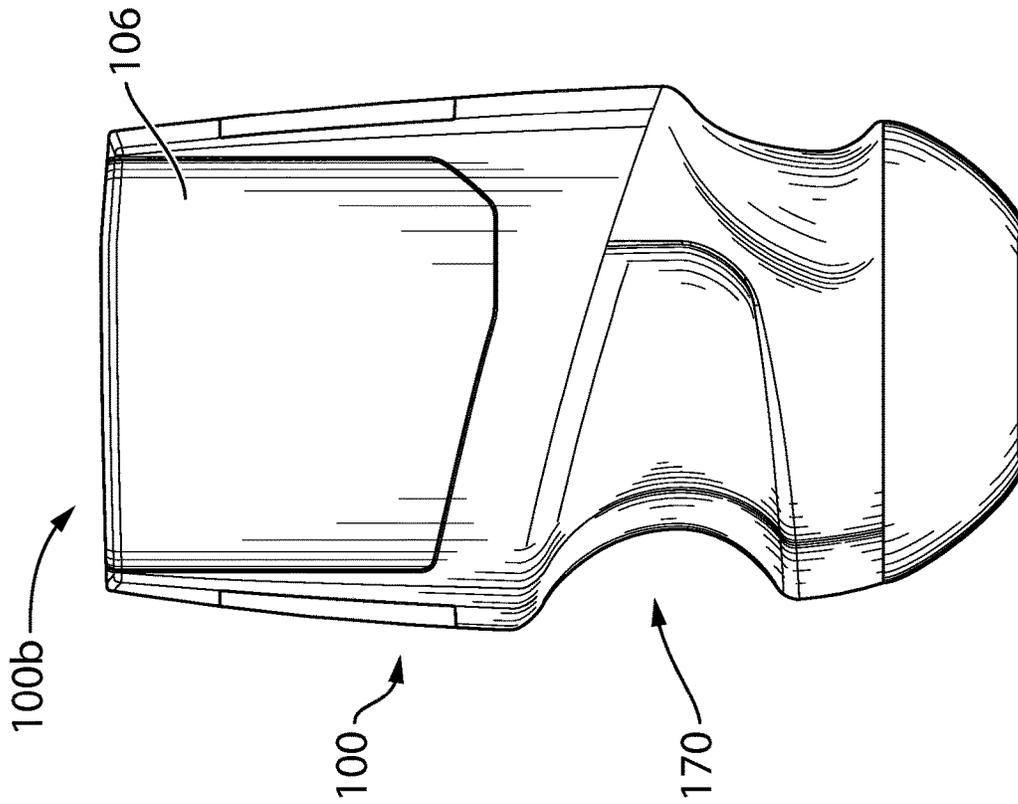


FIG. 1B

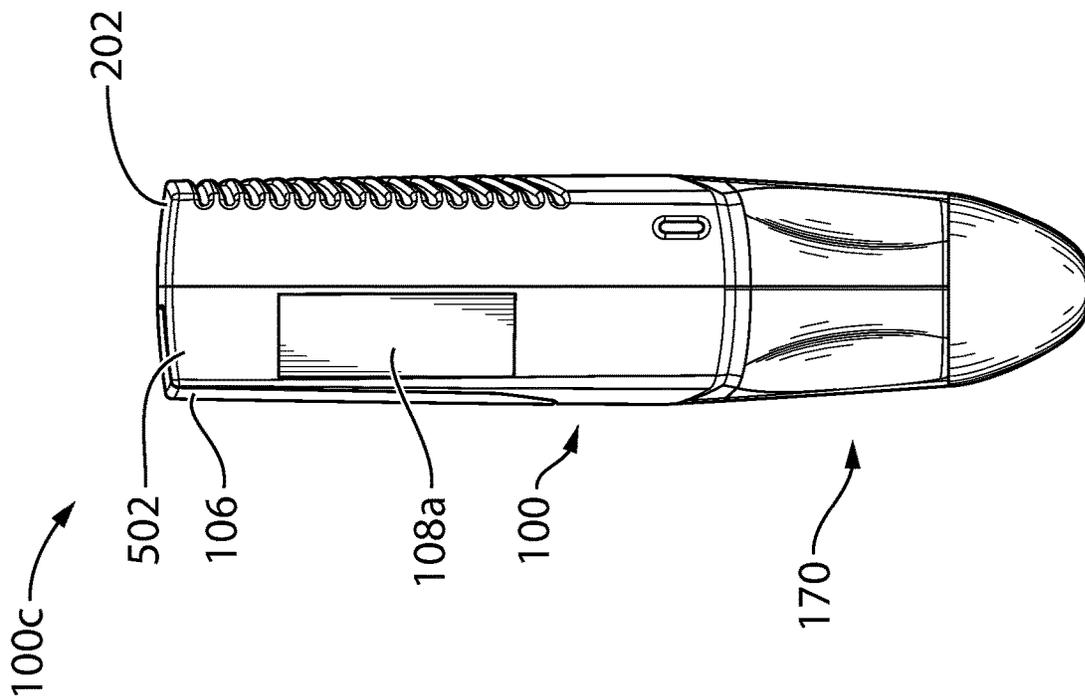


FIG. 1C

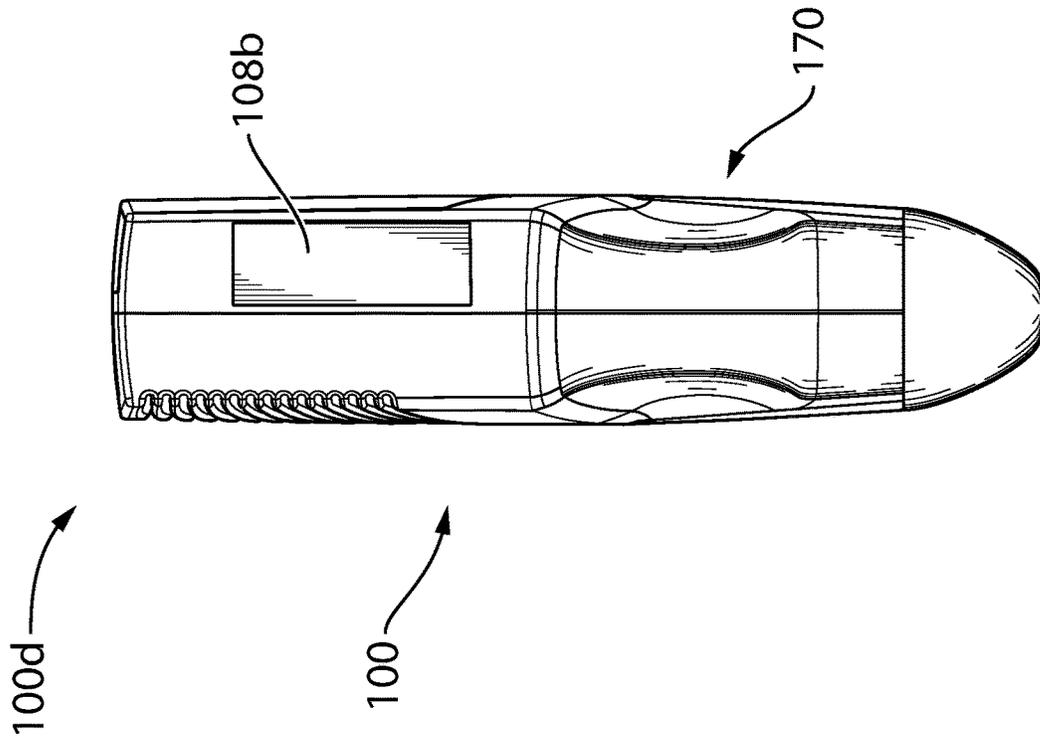


FIG. 1D

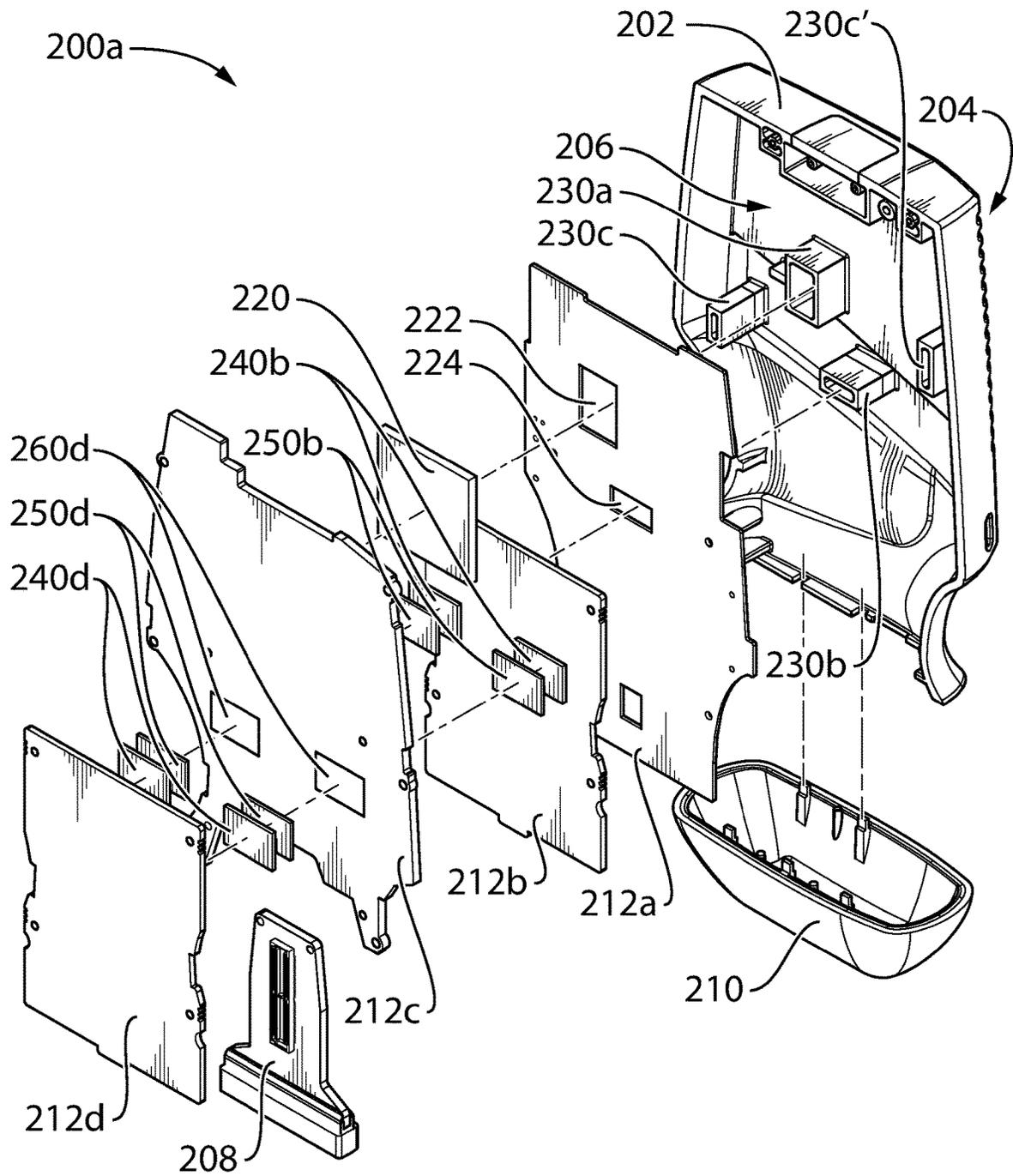


FIG. 2A

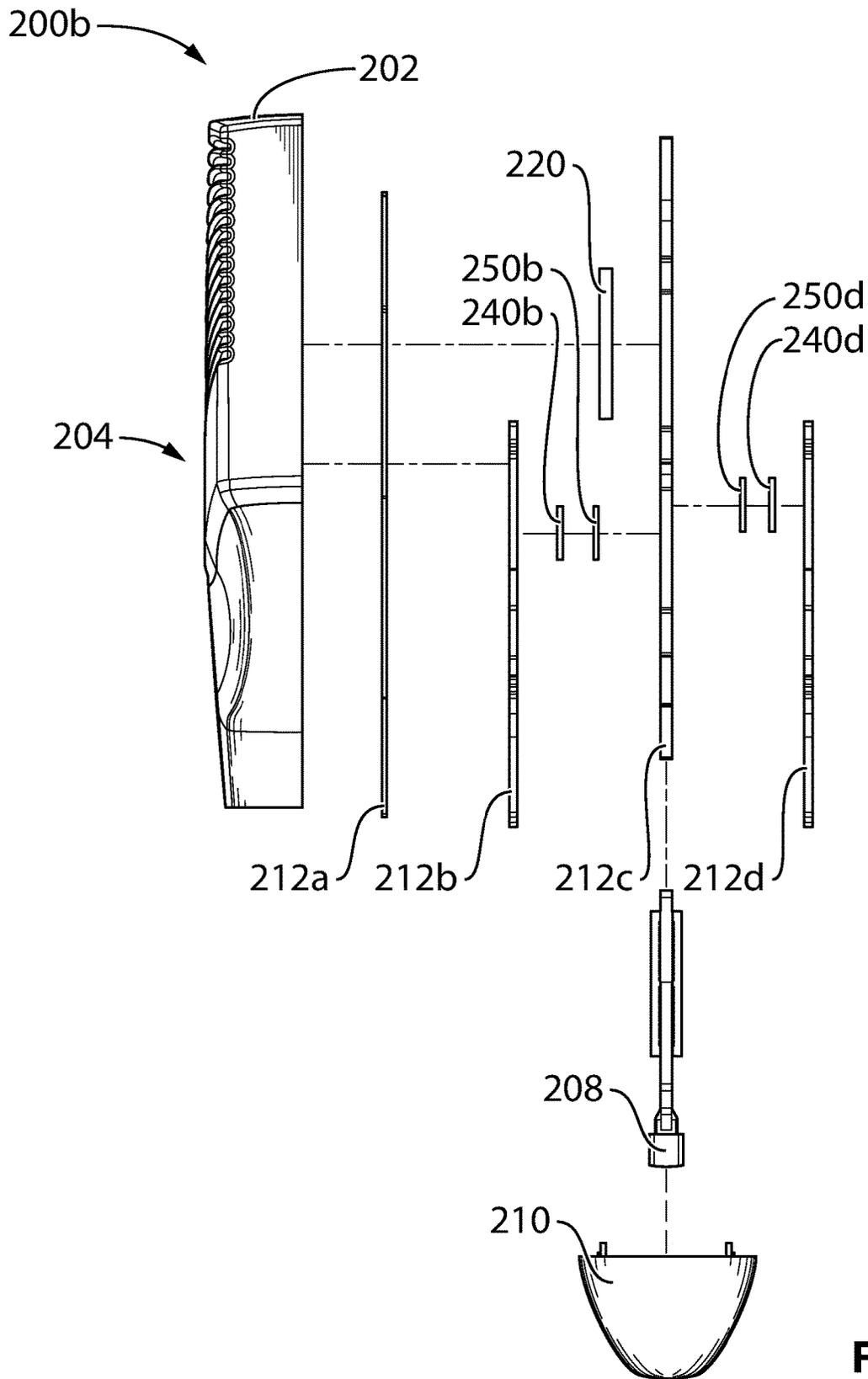


FIG. 2B

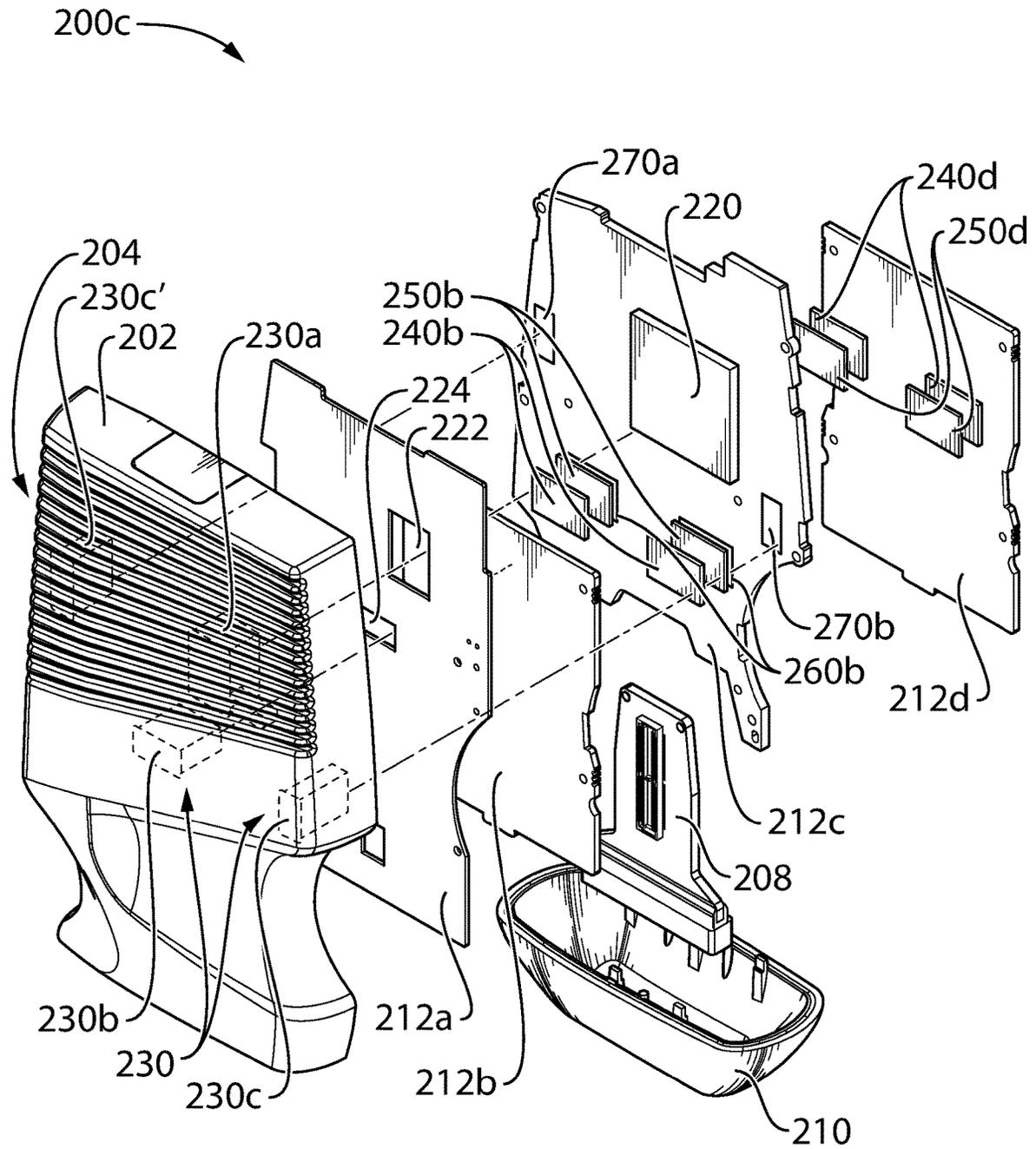


FIG. 2C

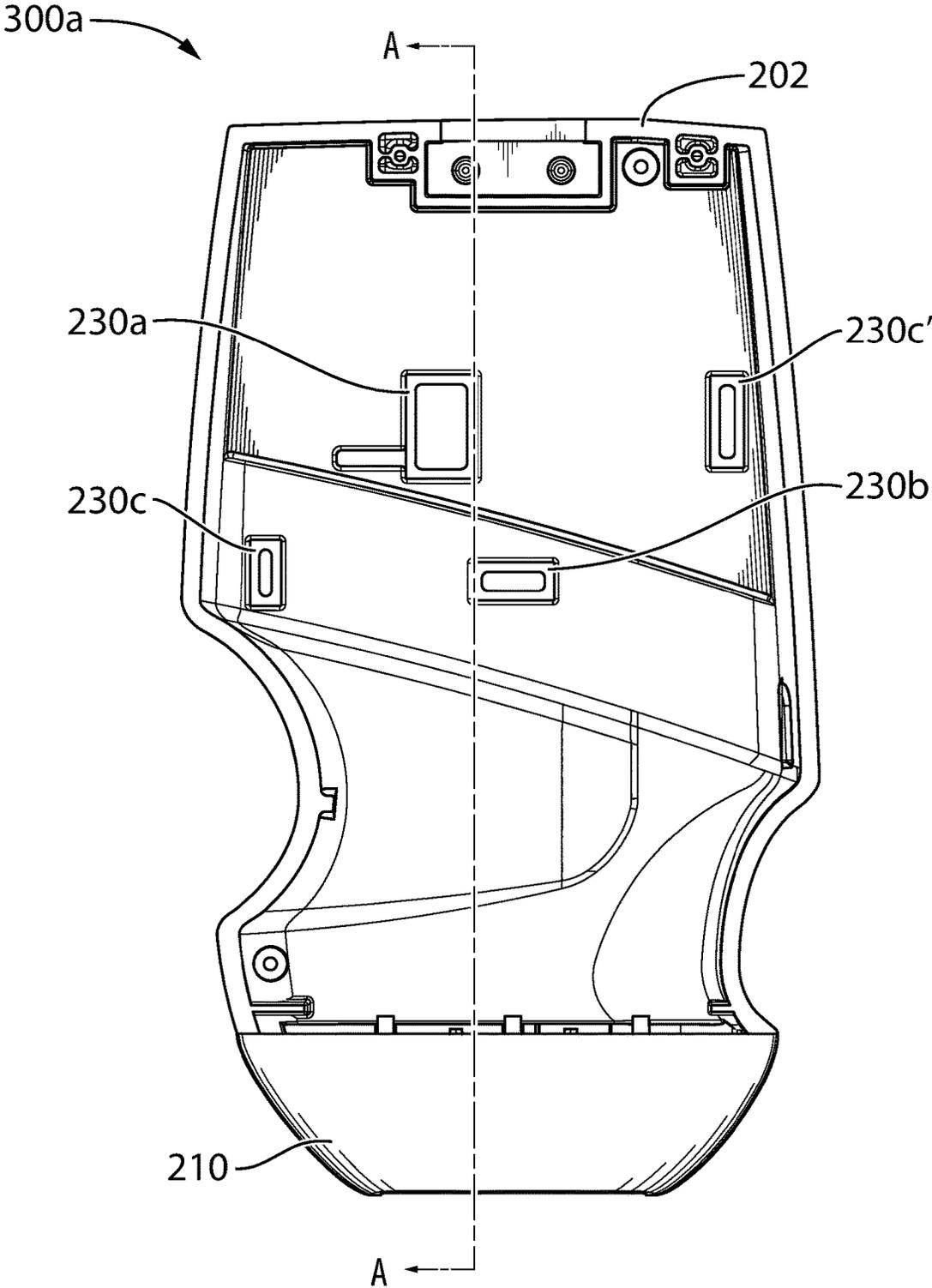


FIG. 3A

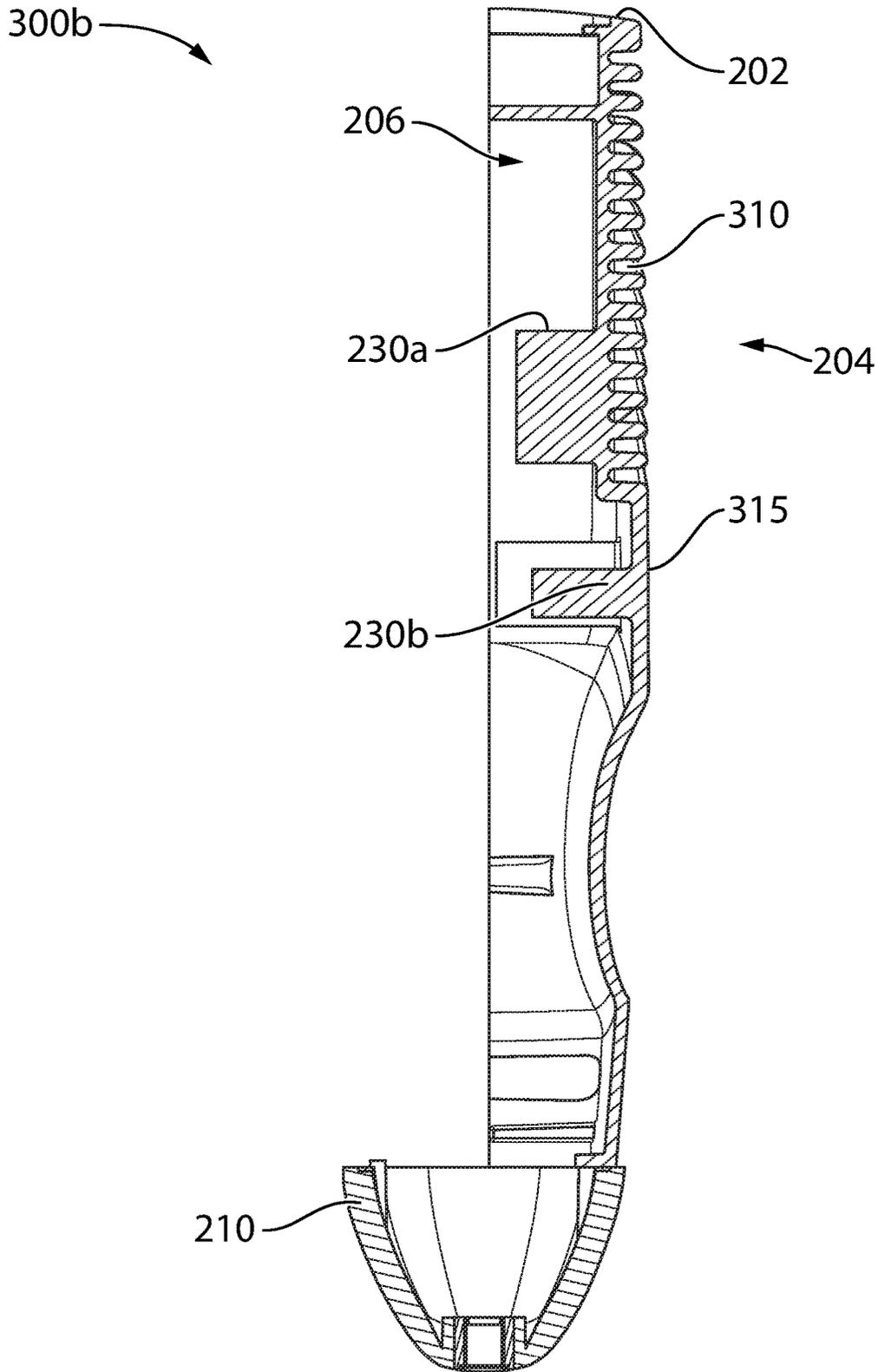


FIG. 3B

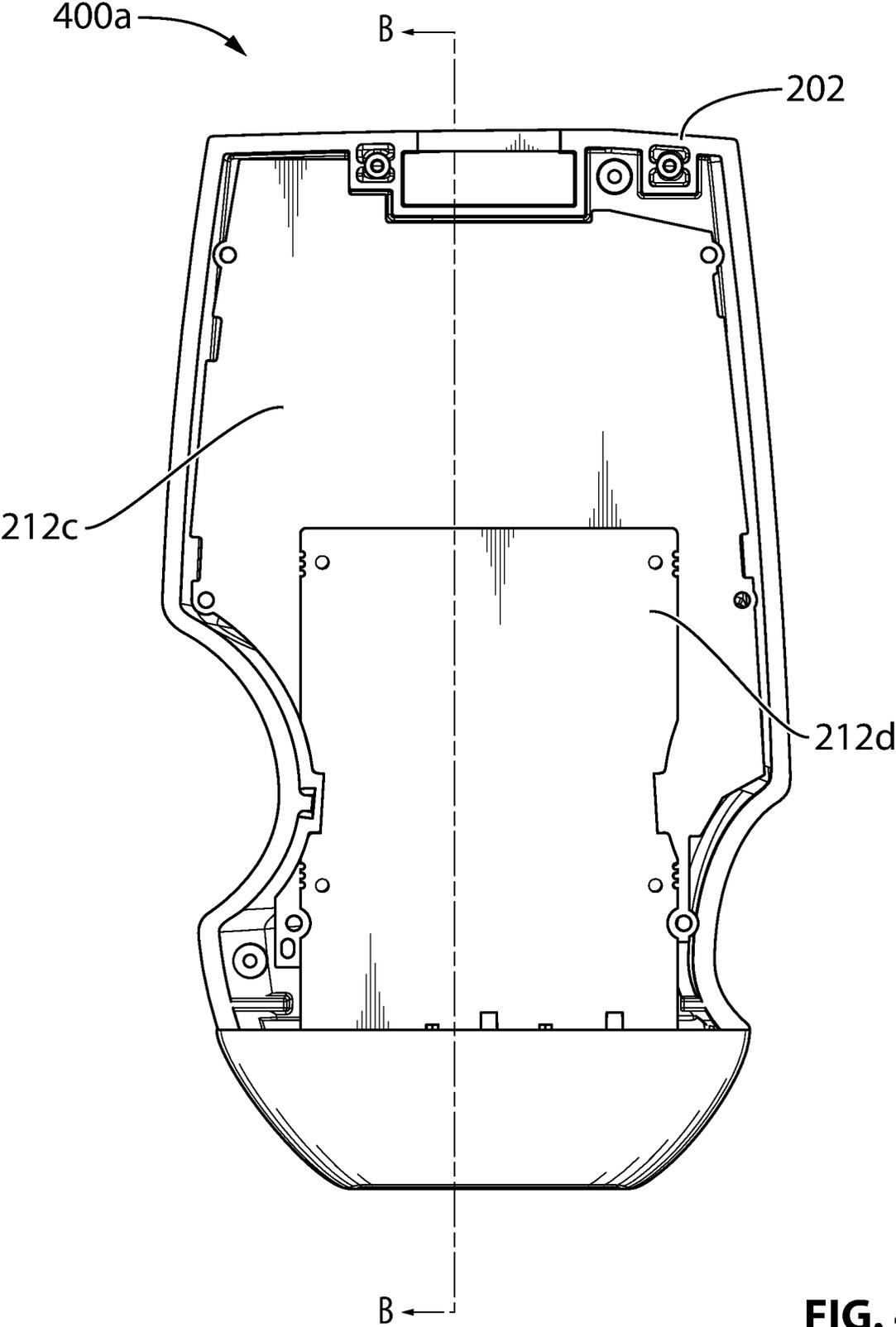


FIG. 4A

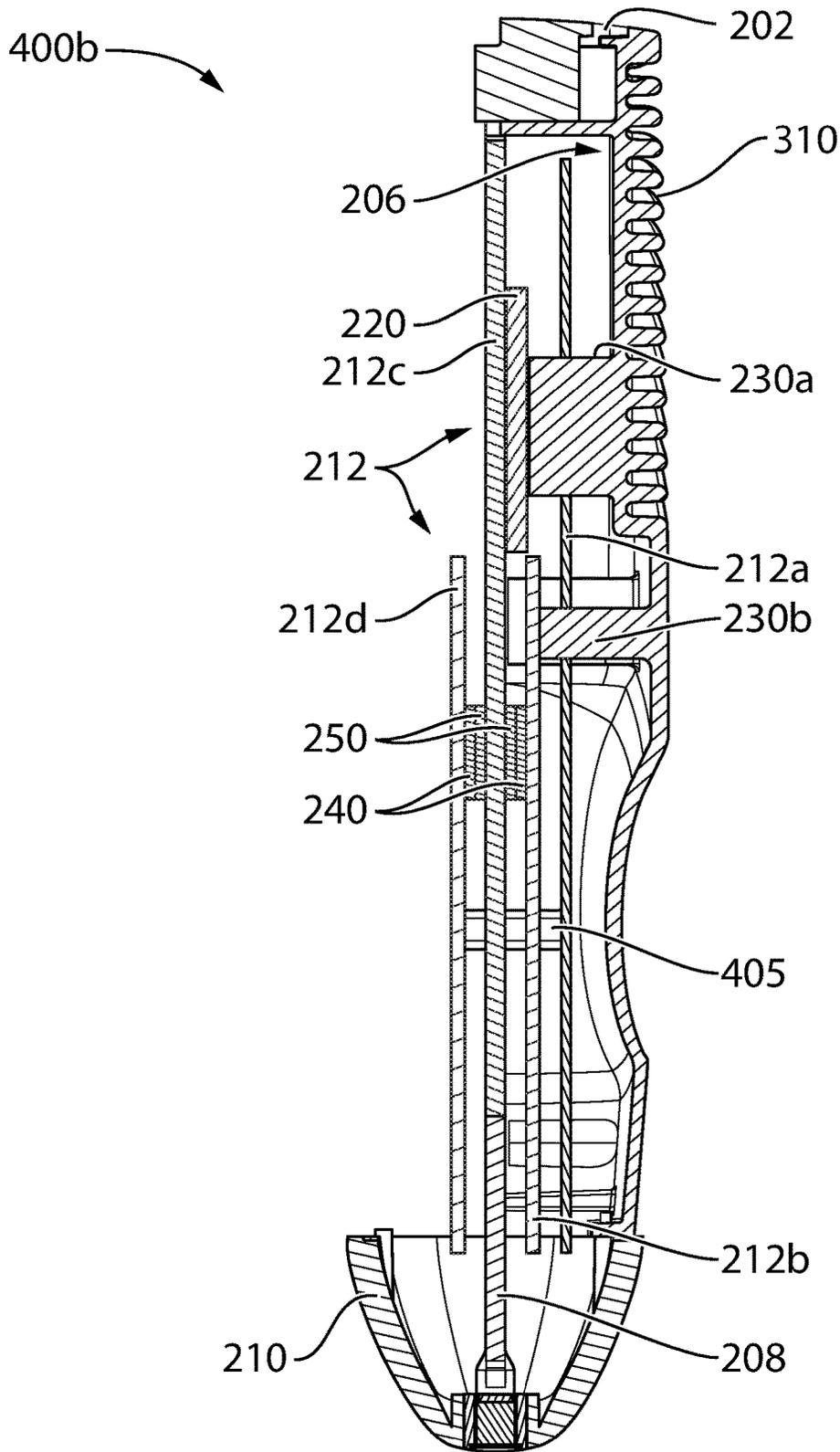


FIG. 4B

500a

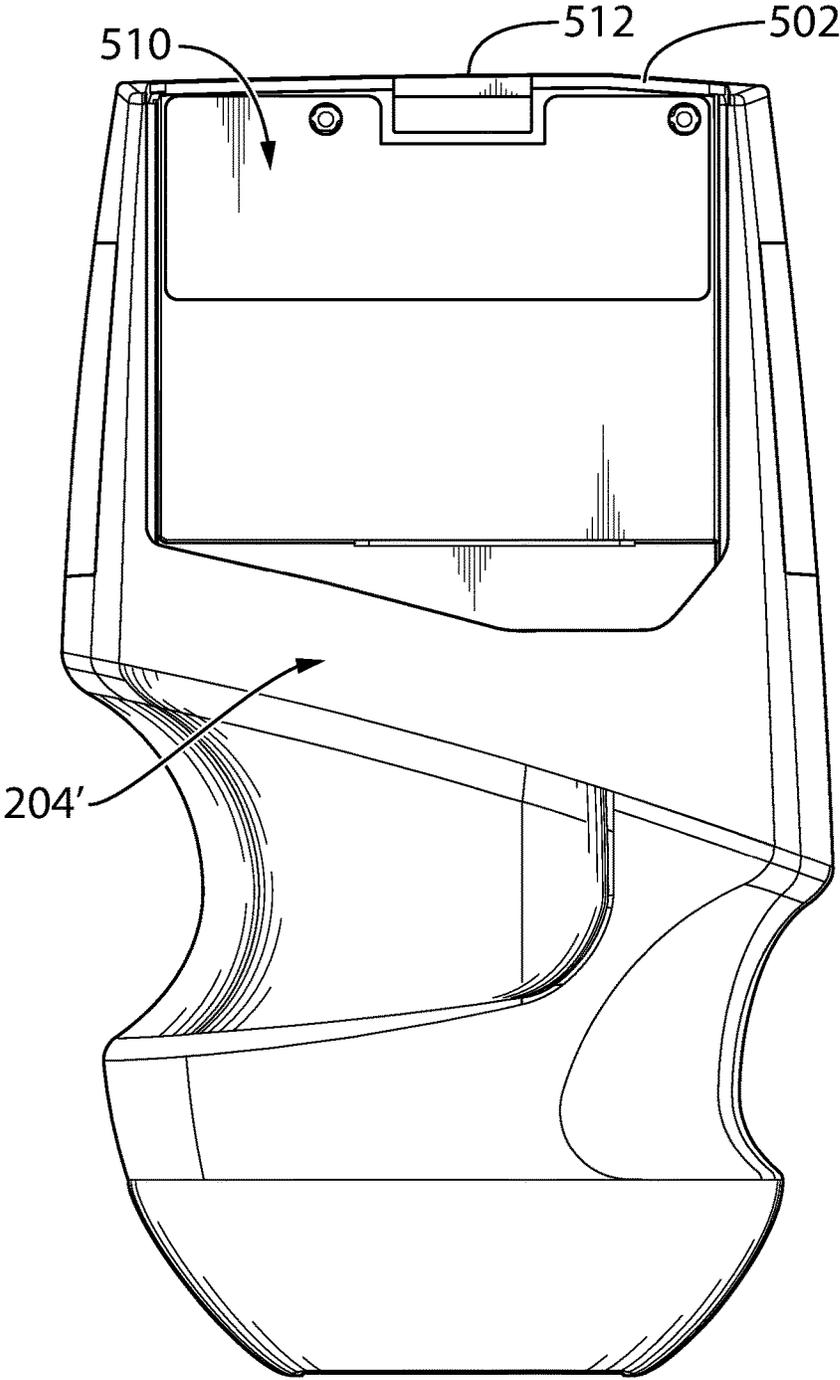


FIG. 5A

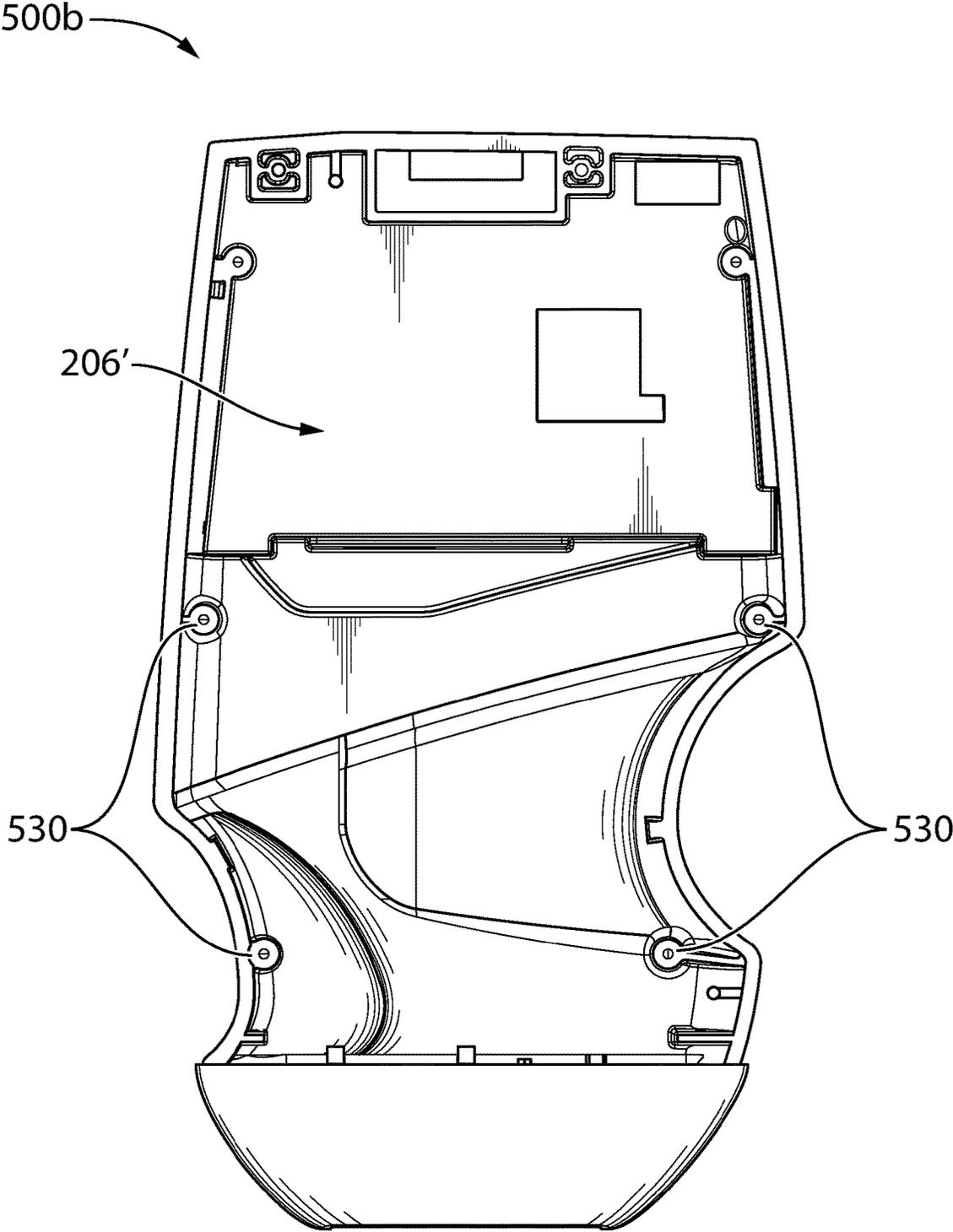


FIG. 5B

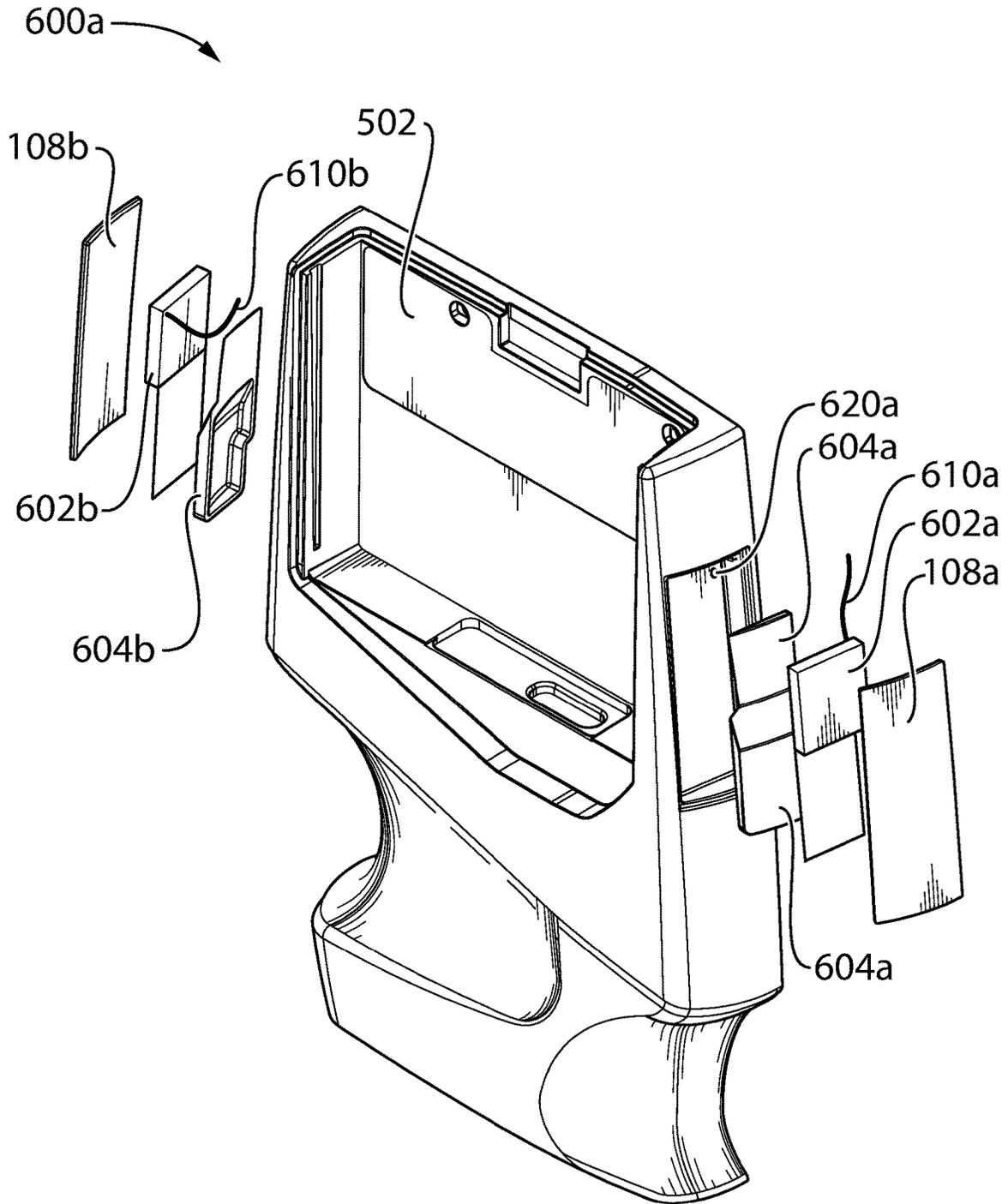


FIG. 6A

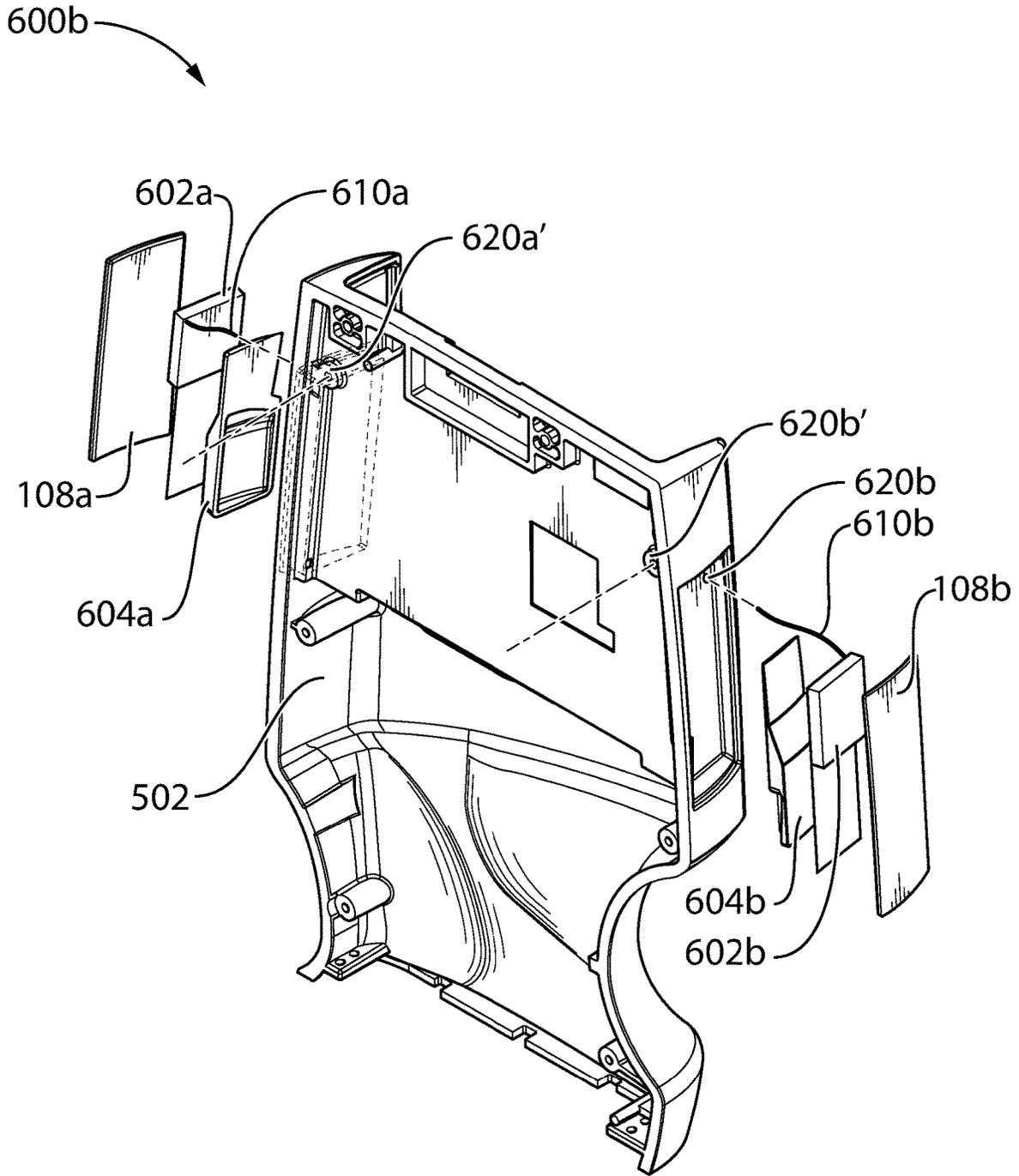


FIG. 6B

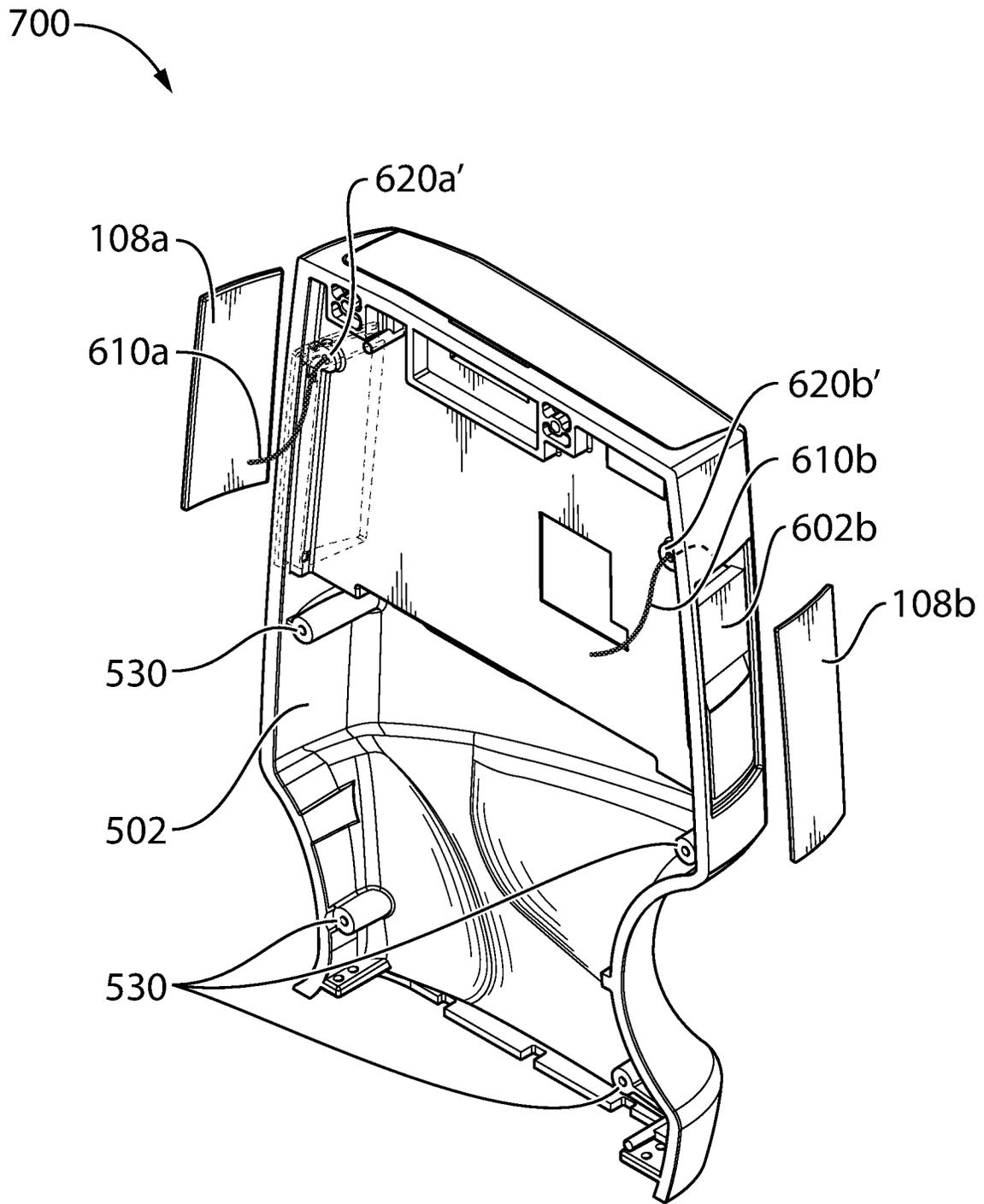


FIG. 7

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ULTRASOUND APPARATUS WITH IMPROVED HEAT DISSIPATION AND METHODS FOR PROVIDING SAME

FIELD

The present disclosure relates generally to ultrasound imaging apparatus, and in particular, ultrasound imaging apparatus with improved heat dissipation properties and related methods.

BACKGROUND

Ultrasound imaging systems may generate heat during operation. For example, heat may be generated from the transducer elements in a transducer array when they are activated to transmit ultrasound signals. Also, heat may be generated by integrated circuits (ICs) that drive the transducer array and process imaging data. For example, these ICs may include Analog to Digital Converters (ADCs) that convert the received ultrasound signals into ultrasound images, and/or other ICs (such as graphics processors).

When imaging tissue, ultrasound probes (also called ultrasound transducers) are typically placed against the skin of a patient. To prevent patient injury or discomfort due the probe head having overly high temperatures, there exist regulations that require surfaces of an ultrasound probe to not exceed certain predetermined temperatures while scanning a patient (e.g. International Electrotechnical Commission (IEC) standard 60601 requires external surfaces of an ultrasound probe to not exceed 48° C. in certain conditions).

In a traditional wired ultrasound system, an ultrasound probe may be connected by a cable or wire to a separate ultrasound processing body. Some traditional heat dissipation techniques attempt to channel heat into and through the cable so that it may be dissipated from the cable and/or through the processing body. Such techniques may be particularly effective in wired ultrasound systems because a number of the heat generating components (e.g., the ICs) can be placed within the ultrasound processing body, so as to reduce the amount of heat that needs to be dissipated from the ultrasound probe.

In a wireless ultrasound system, more of the ICs may need to be included within a single wireless ultrasound imaging apparatus or device. Without a cable through which heat can be transferred, wireless ultrasound systems generally have higher heat dissipation requirements. Moreover, to be able to provide high quality ultrasound images, the processing components may operate with heavy loads and/or high frequencies; this further increases the heat generated by a wireless ultrasound imaging device. Despite the higher heat dissipation requirements, wireless ultrasound devices still have to comply with the regulations that require surfaces of an ultrasound probe to not exceed a given temperature.

There is thus a need for ultrasound imaging apparatus with improved heat dissipation properties and related methods.

BRIEF DESCRIPTION OF THE DRAWINGS

Non-limiting examples of various embodiments of the present disclosure will next be described in relation to the drawings, in which:

FIGS. 1A-1D show front, rear, and side views of an ultrasound imaging device, in accordance with at least one embodiment of the present invention;

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FIG. 2A shows a rear perspective exploded view of some of the components in the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention;

FIG. 2B shows a side exploded view of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention;

FIG. 2C shows a front perspective exploded view of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention;

FIG. 3A shows an interior view of the front shell that forms part of the housing of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention;

FIG. 3B shows a cross-sectional view of the front shell of FIG. 3A, along line A-A shown in FIG. 3A, in accordance with at least one embodiment of the present invention;

FIG. 4A shows a rear view of a partially-assembled ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention;

FIG. 4B shows a cross-sectional view of the partially-assembled ultrasound imaging device shown in FIG. 4A along the line B-B, in accordance with at least one embodiment of the present invention;

FIGS. 5A-5B show exterior and interior views of the rear shell that forms part of the housing of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention;

FIG. 6A shows an exterior perspective exploded view of the rear shell shown in FIGS. 5A-5B, in accordance with at least one embodiment of the present invention;

FIG. 6B shows an interior perspective exploded view of the rear shell shown in FIGS. 5A-5B, in accordance with at least one embodiment of the present invention; and

FIG. 7 shows an interior perspective view of a partially-assembled configuration of the components shown in FIGS. 6A-6B, in accordance with at least one embodiment of the present invention.

DETAILED DESCRIPTION

In a first broad aspect of the present disclosure, there is provided an ultrasound imaging apparatus, including: a housing enclosing a transducer array and at least one integrated circuit (IC) for driving the transducer array during operation of the ultrasound imaging apparatus, wherein the housing includes an interior surface and an exterior surface, and the housing is made substantially of metal; wherein a post is disposed between the at least one IC and the interior surface of the housing, the post being coupled directly to the interior surface of the housing so that heat generated from the at least one IC is transferred via the post to the housing and dissipated via the exterior surface.

In some embodiments, the post is made of the metal. In some embodiments, the post is coupled directly to the at least one IC. In some embodiments, the post is in indirect physical contact with the at least one IC through at least one or more intermediate circuit boards.

In some embodiments, the ultrasound imaging apparatus further includes a circuit board having: a surface facing the interior surface of the housing, and a surface not facing the interior surface of the housing, and the at least one IC is coupled directly to the surface of the circuit board not facing the interior surface of the housing; wherein the post is coupled directly to an area on the surface of the circuit board facing the interior surface of the housing, the area being proximately opposite the at least one IC.

In some embodiments, the thermal conductivity of the housing is at least 55 watts per meter kelvin (W/(m·K)). In some embodiments, the density of the metal or material forming the housing is less than 5 grams per cubic centimeter (g/cm³).

In some embodiments, the post and the housing form part of a unitary body, and the unitary body is created by at least one of: injection moulding, die casting, and machining. In some embodiments, the post is formed separately from the housing, and the post is attached to the interior surface of the housing.

In some embodiments, the housing includes a grip portion and the grip portion is covered with a polymer-based material.

In some embodiments, the exterior surface of the housing includes a plurality of fins. In some embodiments, the fins are made of the metal. In some embodiments, the plurality of fins increases a surface area of the exterior surface of the housing by at least 30%.

In some embodiments, the plurality of fins are positioned on a region of the exterior surface opposite a location on the interior surface that is directly coupled to the post.

In some embodiments, the region of the exterior surface having the plurality of fins have a first size and the location on the interior surface that is directly coupled to the post has a second size, and the first size is larger than the second size.

In some embodiments, the ultrasound imaging device further includes a first side of the ultrasound imaging apparatus and a second side of the ultrasound imaging apparatus opposite the first side, and wherein the fins are positioned on the first side of the ultrasound apparatus and a battery for powering the ultrasound imaging apparatus is positioned on the second side of the ultrasound imaging apparatus.

In some embodiments, the exterior surface of the housing has a surface area of at least 10,000 square millimeters (mm²).

In some embodiments, the at least one IC consumes at least 3 watts of power while imaging.

In some embodiments, the housing protects from ingress into an interior of the ultrasound imaging apparatus, and the housing has an International Protection Marking of at least IPX7.

In some embodiments, the housing includes an opening that allows for the at least one IC to connect to an antenna positioned on the exterior surface of the housing.

In another broad aspect of the present disclosure, there is provided a method of facilitating dissipation of heat in an ultrasound imaging apparatus, the method including: providing a housing for the ultrasound imaging apparatus, the housing enclosing a transducer array and at least one integrated circuit (IC) for driving the transducer array during operation of the ultrasound imaging apparatus, wherein the housing includes an interior surface and an exterior surface, and the housing is made substantially of metal; and activating the at least one IC during operation of the ultrasound imaging apparatus, wherein heat generated from the at least one IC is transferred to the housing and dissipated by the exterior surface via at least one post that is disposed between the at least one IC and the interior surface of the housing, the post being coupled directly to the interior surface of the housing.

In some embodiments, the exterior surface of the housing includes a plurality of fins.

In another broad aspect of the present disclosure, there is provided a housing for an ultrasound imaging apparatus, the housing for enclosing a transducer array and at least one

integrated circuit (IC) for driving the transducer array during operation of the ultrasound imaging apparatus, the housing including: an interior surface configured to receive a post, the post being positionable between the at least one IC and the interior surface of the housing; and an exterior surface, wherein heat generated from the at least one IC is transferable via the post to the housing and the heat is dissipated via the exterior surface.

For simplicity and clarity of illustration, where considered appropriate, reference numerals may be repeated among the figures to indicate corresponding or analogous elements or steps. In addition, numerous specific details are set forth in order to provide a thorough understanding of the exemplary embodiments described herein. However, it will be understood by those of ordinary skill in the art that the embodiments described herein may be practiced without these specific details. In other instances, certain steps, signals, protocols, software, hardware, networking infrastructure, circuits, structures, techniques, well-known methods, procedures and components have not been described or shown in detail in order not to obscure the embodiments generally described herein.

Furthermore, this description is not to be considered as limiting the scope of the embodiments described herein in any way. It should be understood that the detailed description, while indicating specific embodiments, are given by way of illustration only, since various changes and modifications within the scope of the disclosure will become apparent to those skilled in the art from this detailed description. Accordingly, the specification and drawings are to be regarded in an illustrative, rather than a restrictive, sense.

Referring to FIGS. 1A-1D shown there generally as **100a**, **100b**, **100c**, **100d** respectively are front, rear, left side, and right side views of an ultrasound imaging device, in accordance with at least one embodiment of the present invention. FIG. 1A shows the front view of the ultrasound imaging device **100**. The ultrasound imaging device **100** generally has a housing **102** which contains a transducer array and the processing components. The transducer array may be positioned near a bottom portion **104** of the housing **102**. As the ultrasound imaging device **100** is used to perform imaging, heat may be generated by the transducer array and/or the processing components within the housing **102**. In various embodiments, a grip portion **170** may be provided (e.g., to facilitate easier holding of the ultrasound imaging device **100**). In the specific example embodiment illustrated, the grip portion **170** may be shaped in a manner that (alone or in combination with other visual elements) primarily provides a distinctive visual and decorative appearance for the ultrasound imaging device **100**.

FIG. 1B shows the rear view of the ultrasound imaging device **100**. In the illustrated embodiment, an upper portion of the rear portion of the housing **102** may hold a removable battery **106** for powering the ultrasound imaging device **100**. In various embodiments, the shape, positioning, and appearance of the battery **106** when it is secured to the ultrasound imaging device **100** may take different forms. However, in the example embodiment illustrated, the shape of the battery **106** and its appearance when it interfaces with the ultrasound imaging device **100** primarily provides (alone or in combination with other visual elements) a distinctive visual and decorative appearance for the ultrasound imaging device **100**. As illustrated, the grip portion **170** may be shaped to extend to the rear of the ultrasound imaging device **100**.

FIG. 1C shows a left side view of an example embodiment of an ultrasound imaging device **100**. The housing **102** may be made up of a front shell **202** that mates with a rear

shell **502**. Shown also in FIG. **1C** is the removable battery **106** in the attached position. To allow for improved heat dissipation, the housing **102** may be made substantially of metal.

For example, the metal may be made of aluminum or magnesium, and/or a related alloy or composite. In some embodiments, the housing **102** is made of a magnesium composite having at least 50% magnesium. In some embodiments, the magnesium alloy AZ91D is used to form some or all of the housing **102**. Additionally or alternatively, in some embodiments, the magnesium alloy AZ31B may be used to form some or all of the housing **102**. Further, in some embodiments, aluminum 6061 may be used to form some or all of the housing **102**.

The thermal conductivity characteristics of materials can be used as a way to identify a suitable material to form the housing **102**. For example, aluminum 6061 may have a relatively high thermal conductivity of 167 watts per meter kelvin (W/(m·K)), whereas the noted magnesium alloys may generally have lower thermal conductivity (e.g., AZ91D has thermal conductivity of 72.3 W/(m·K), and AZ31B has thermal conductivity of 96 W/(m·K)). Thus, in some embodiments, aluminum 6061 may be selected for the material to be used to form the housing **102** (e.g., if optimal thermal performance is desired).

However, in additional embodiments, it may be possible to select the material for the housing **102** not solely upon thermal performance but also upon additional characteristics of the material such as density (which may affect the overall weight of the ultrasound imaging device **100**) and/or the suitability of the material for mass production processes such as die casting. For example, whereas aluminum 6061 may provide optimal thermal conductivity performance, aluminum 6061 also has a higher density at 2.71 grams per cubic centimeter (g/cm³). In contrast, the noted magnesium alloys generally have lower thermal conductivity performance, but also a lower density (e.g., AZ91D has a density of 1.9 g/cm³, and AZ31B has a density of 1.77 g/cm³). In embodiments where it is desirable to find a balance between a material that provides sufficient thermal conductivity and also does not unduly increase the overall weight of ultrasound imaging device **100**, the noted example magnesium alloys may be used. For example, it may be desirable to select AZ91D over aluminum 6061 because the reduction of the density from 2.71 g/cm³ to 1.9 g/cm³ provides roughly a 30% decrease in the weight of the housing **102**, while still providing acceptable thermal conductivity performance. Overall, the thermal conductivity of the material selected to form the housing **102** may be at least 55 W/(m·K) and/or the density of the material selected to form the housing may be less than 5 g/cm³.

With respect to suitability for mass production processes, it will be understood by persons skilled in the art that there may be multiple ways of producing the parts (e.g., the front shell **202** and/or rear shell **502**) that form the housing **102**. For example, it may be possible to machine the parts (e.g., use a piece of raw material and cut it into a desired final shape and size using a controlled material-removal process such as a Computer Numeric Control (CNC) automated machine). Alternatively, it may be possible to create the part using die casting (e.g., to form the part by pouring molten metal into a mold), which is typically used for mass production. As between the different example magnesium alloys discussed herein, AZ91D may be more suitable for die casting over AZ31B (which is more suitable for machining); although any one or more of machining, injection moulding,

die casting, or any other suitable production method may be used for providing the parts for the housing **102**.

Traditional ultrasound probes are typically constructed with a housing made substantially of heat insulating material (e.g., a polymeric material such as plastic). This is to prevent surfaces of the ultrasound probe from experiencing high temperatures, so as to be non-compliant with regulations that require external surfaces of an ultrasound probe to be lower than a predetermined temperature. In such probes, heat is primarily channeled towards the non-imaging end of the ultrasound probe, where there is a cable through which the heat can be transferred and dissipated (e.g., in a wired ultrasound system) or where there is a localized heatsink for absorbing and/or dissipating the heat.

In the present embodiments, a substantial portion of the housing **102** is made of metal (except for the transducer array cap **210** (as shown in FIGS. **2A-2C**)). This allows almost the entire surface area of the ultrasound imaging device **100** to act as a heatsink and dissipate heat. This larger surface area may dissipate more heat than any localized heatsink, so as to lower the overall heat retained in the ultrasound imaging device **100**. In turn, this reduces the likelihood that any single exterior surface of the ultrasound imaging device **100** (or region thereof) would experience overly high temperatures that would cause non-compliance with applicable regulations.

For example, in the embodiments discussed herein, a significant portion of the heat may be generated by ICs (e.g., the ADCs and graphic processors) provided within the housing **102**; and as discussed below, posts may be added to extend from an interior surface of the housing **102** to assist with drawing heat away from the ICs towards the exterior surface of the housing **102** for improved heat dissipation. Due to the heat generated by the ICs, traditional ultrasound transducer designs may generally avoid the use of metal on the exterior surface of the housing **102** because metal may be warmer to the touch (and thus be more vulnerable to non-compliance with applicable regulations) than other materials such as plastic. However, by having a substantial portion of the housing **102** be made of metal, the heat generated by the ICs may be able to be spread more evenly throughout the housing **102**. As a result, the present embodiments may be less likely to experience any localized hotspots that make the device non-compliant with applicable regulations.

In some embodiments, substantially all of the exterior surface of the metallic housing **102** may be exposed to air. In alternative embodiments, certain parts of the housing **102** may be selectively covered with a layer of rubber or similar material. For example, in some embodiments, the grip portion **170** may be covered with a thin layer of rubber. The rubber material may make the ultrasound imaging device **100** less slippery and easier to grip. Additionally, by targeting a limited area of the overall metallic housing **102** to be covered with the rubber material, such embodiments limit the insulating impact of the rubber cover to the targeted area (e.g., the grip portion **170**) while still allowing a significant portion of the remaining metallic housing **102** to be exposed to air for enhanced heat dissipation. Further, the rubber cover on the grip portion **170** may reduce the heat sensation felt by ultrasound operators and allow operators to hold the device for longer periods of time. In doing so, the hand holding the ultrasound imaging device **100** may serve as a heat sink (e.g., a heat sink additional to the heat radiating into the ambient air from the remaining exposed metal portions of the housing **102**) for longer periods.

In various embodiments, the percentage of the total exterior surface area of the metal housing **102** covered by the rubber layer may be 0%-49%. For example, in the illustrated example embodiments, the overall surface area of the metallic housing **102** may be approximately 31,525 millimeters squared (mm²). However, the surface area of the grip portion **170** may be approximately 12,164 mm², so that the remaining non-rubber-covered surface area of the metallic housing **102** is approximately 19,361 mm². In this embodiment, the rubber-covered grip portion **170** thus constitutes approximately 38.6% of the external surface area of the housing **102**, while the non-rubber covered portion of the housing **102** constitutes substantially more than half of the remaining exposed surface of the metallic housing **102** (e.g., approximately 61.4% of the surface area of the housing **102**). It will be understood by persons skilled in the art that other configuration of targeted rubber covering of selected portions of the housing **102** are possible. For example, an ultrasound imaging device **100** configured with a smaller grip portion **170** may have a smaller percentage of the overall surface area of the housing **102** be covered by rubber. While the use of a rubber covering is discussed herein, in various embodiments, the cover may be made of any suitable polymer-based material. For example, any one or more of polyurethane, thermoplastic elastomer, and/or silicone may be used in addition to, or instead of, rubber as the material for the covering.

Moreover, the embodiments described herein may include other configurations of ultrasound imaging devices with metal housings **102** that have a variety of different surface area measurements, so long as the heat dissipation techniques described herein are practised. For example, in some embodiments, the exterior surface of the metal housing **102** of an ultrasound imaging device **100** may have a surface area of at least 10,000 mm².

Referring still to FIG. 1C, a recess may be provided on an exterior surface of the housing **102** to allow for placement of an antenna that allows for wireless communications. As shown, a recess is provided under a cover **108a**, under which suitable antennas for wireless communications may be placed. In some embodiments, to allow for improved wireless communication performance and/or capacity, the housing **102** may be provided with multiple recesses to allow for placement of multiple antennas. FIG. 1D shows a right side view of the ultrasound imaging device **100**, which has a recess similar to that which is on the left side of the ultrasound imaging device **100** and is covered by a cover **108b**. The grip portion **170** is also shown in FIGS. 1C and 1D. Further details of the placement of the antenna within the recesses are discussed below in relation to FIGS. 6A, 6B, and 7.

Referring to FIG. 2A, shown there generally as **200a** is a rear perspective exploded view of some of the components in the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention. As shown, the front shell **202** (forming part of the housing **102** shown in FIG. 1A) may have an exterior surface **204** and an interior surface **206**. A number of posts **230a**, **230b**, **230c**, **230c'** may be coupled directly to the interior surface **206** of the front shell **202** to allow heat generated by ICs to be transferred via the posts **230a**, **230b**, **230c**, **230c'** to the housing **102** and dissipated via the exterior surface **204**. As shown, the exterior surface **204** may be exposed to open air (e.g., without any covering) to facilitate improved heat dissipation.

In the illustrated embodiment, there may be a number of circuit boards **212a**, **212b**, **212c**, **212d** which form an

assembly and can be mated with the front shell **202**. The transducer array **208** may be coupled to the circuit boards **212a**, **212b**, **212c**, **212d**, and in completely assembled from, the transducer array **208** may be covered with a transducer cap **210**.

As shown with dotted connection lines in FIG. 2A, the circuit board **212a** may be provided with openings **222**, **224** or cut-outs that fit around the posts **230a**, **230b**, **230c**, **230c'**. For example, the opening **222** may be shaped so as to fit around post **230a**, and opening **224** may be shaped to fit around post **230b**. The post **230a** may then have direct physical contact with an IC (e.g., processor **220**) provided on circuit board **212c**. In some embodiments, thermal paste may be provided on the processor **220** to increase the thermal coupling between the processor **220** and the post **230a**. Thermal paste or grease may be usable in various scenarios described herein. An example thermal grease that can be used herein is Hydronaut™ thermal paste available from Thermal Grizzly™. However, it will be understood that any other suitable thermal paste or grease may be used instead.

To convert the analog ultrasound information received by the ultrasound transducer **208** into digital signals, a number of ADCs **240b**, **240d** may be positioned on circuit boards **212b**, **212d** respectively. As shown, the ADCs **240b** are provided on the surface of the circuit board **212b** which faces circuit board **212c**.

The ADCs **240b** may heat up the upper region of circuit board **212b**. To provide improved dissipation of the heat present on the upper region of circuit board **212b**, the post **230b** may mate with an area on the surface of the circuit board **212b** that is opposite the ADCs **240b** and facing the interior surface **206** of the front shell **202**. As illustrated with dotted connection lines, the post **230b** may protrude through opening **224** in circuit board **212a** to mate with an area of the upper region of board **212b** that is proximately opposite the ADCs **240b**. However, in alternative embodiments, the post **230b** may be configured to mate to circuit board **212b** at an area that is directly opposite the ADCs **240b** (e.g., if the position of the ADCs **240b** are moved towards the top of the circuit board **212b** or if the post **230b** and the opening **224** is moved lower to mate with an area on the surface of the circuit board **212b** that is directly opposite the ADCs **240b**). Similar to the post **230a**, the post **230b** mating with circuit board **212b** helps to draw heat away from the upper region of the circuit board **212b** (which, in turn, may experience high temperatures due to the heavy loads being processed by the ADCs **240b**) towards the front shell **202** for dissipation through the exterior surface **204**. In some embodiments, thermal paste may also be used to improve the thermal coupling between the post **230b** and where it mates with the surface of the circuit board **212b** facing the front shell **202**.

Configuring posts **230** to couple directly to a heat source such as an IC (as is the case for post **230a**) may generally be considered the most efficient way to draw heat away from the IC. While introducing an intermediate medium such as a circuit board **212b** in between the heat source (e.g., ADCs **240b**) and the post **230b** may slightly reduce the efficiency of the heat transfer, the degradation in heat transfer efficiency may be minimal in embodiments where the ultrasound imaging device **100** is small and enclosed. For example, this may be because the small and enclosed nature of the ultrasound imaging device **100** will cause the temperature of almost all the components within the housing **102** to reach a similar level in a relatively short period of time. This may enable the circuit board **212b** to transfer heat

to the post **230b** with a thermal transfer efficiency that is similar to scenarios where the ICs are coupled directly to a post **230**.

To further improve the dissipation of heat generated by ADCs **240b**, the ADCs **240b** may mate directly with portions of the circuit board **212c** (shown with dotted connection lines in FIG. 2A). As discussed in greater detail below with respect to FIG. 2C, heat may transfer through the ground plane of the circuit board **212c** and be transferred to posts **230c**, **230c'**, which may be mated with the circuit board **212c** at another area of the board **212c** other than where the ADC **240b** mates with circuit board **212c**. As with the post **230b**, the posts **230c**, **230c'** helps to transfer the heat generated by the ADCs **240b** to the housing **202** so that it can be dissipated by the exterior surface **204**.

Various techniques may be used to facilitate the mating of ADCs **240b** to the circuit board **212c**. As shown in FIG. 2A, thermal pads **250b** are used to provide coupling and thermal conductivity between the ADCs **240b** and the circuit board **212c**. However, other methods of facilitating thermal coupling (e.g., thermal grease or paste) may also be used. Generally, in various embodiments herein, thermal pads or thermal grease may be used interchangeably. For example, thermal pads may be used to bridge wider gaps, and thermal grease may be used to bridge narrower gaps. However, it will be understood by persons skilled in the art that any combination of one or more of thermal pads, thermal grease, or any other suitable method of providing thermal coupling may be used herein when thermal coupling between components is discussed.

In some embodiments, to provide additional capacity to process received ultrasound signals and provide improved image quality, there may be additional ADCs **240d** on circuit board **212d**. As illustrated, these ADCs **240d** may similarly mate with the circuit board **212c** via thermal pads **250d** to allow for improved dissipation of the heat generated by ADCs **240d**. In FIG. 2A, exposed ground plane areas **260d** on the circuit board **212c** are shown. As shown with the dotted connection lines, the ADCs **240d** may mate to these exposed ground plane areas **260d** via thermal pads **250d** to facilitate the transfer of heat from the ADCs **240d** to the ground plane of circuit board **212c**. Referring briefly simultaneously to FIG. 2C, similar exposed ground plane areas **260b** may be provided on the front surface of circuit board **212c** to allow mating with the ADCs **240b** on the circuit board **212b** via thermal pads **250b**.

Referring to FIG. 2B, shown there generally as **200b** is a side exploded view of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention. Dotted connection lines show how post **230a** (not shown in FIG. 2B) in front shell **202** may mate with processor **220** provided on circuit board **212c** through circuit board **212a**. Similarly, another dotted connection line shows how post **230b** (not shown in FIG. 2B) may mate with a region of the front surface of circuit board **212b** that is proximately opposite the ADCs **240b** which may be provided on circuit board **212b**. Further dotted connection lines show how ADCs **240b** provided on circuit board **212b** may be mated to circuit board **212c** via thermal pads **250b**, and how ADCs **240d** provided on circuit board **212d** may be mated to circuit board **212c** via thermal pads **250d**. The transducer array **208** may be connected to circuit board **212c** and transducer cap **210** are also shown in FIG. 2B. As discussed, the heat generated by the various components ICs may travel through the posts **230** (not shown in FIG. 2B) to be dissipated via exterior surface **204**.

Referring to FIG. 2C, shown there generally as **200c** is a front perspective exploded view of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention. FIG. 2C shows a front view of the front shell **202** of the housing **102** having exterior surface **204**, and internal posts **230a**, **230b**, **230c**, **230c'** shown in dotted outline. FIG. 2C also shows the surfaces of circuit boards **212a**, **212b**, **212c**, **212d** facing the interior surface **206** of the front shell **202**, along with transducer array **208** and transducer cap **210**. In FIG. 2C, the processor **220** is shown as being fixed to circuit board **212c**. As was discussed in relation to FIG. 2A above, a dotted connection line shows how post **230a** may protrude through circuit board **212a** via opening **222** so as to mate directly with processor **220** and draw heat away therefrom. Similarly, another dotted connection line shows how post **230b** may protrude through circuit board **212a** via opening **224** so as to mate with an area on the surface of circuit board **212b** that is proximately opposite ADCs **240b**.

FIG. 2C also shows how ADCs **240b**, **240d** may mate with circuit board **212c** via thermal pads **250b**, **250d** respectively. As was the case with the surface of circuit board **212c** facing away from the interior surface **206** of the front shell **202** (as shown in FIG. 2A), there may be exposed ground plane areas **260b** on the front surface of the circuit board **212c** for mating with the ADCs **240b** on circuit board **212b** via thermal pads **250b**.

As viewable in FIG. 2C, dotted connection lines show how exposed ground plane areas **270a**, **270b** may be provided to mate with posts **230c'**, **230c** respectively. Heat generated by the ADCs **240b**, **240d** may generally be transferred via the thermal pads **250b**, **250d** to the exposed ground plane areas **260b**, **260d**. As will be understood by persons skilled in the art, the ground plane of circuit board **212c** may generally be made of a material that is of high thermal conductivity (e.g., copper). As a result, the heat received by the exposed ground plane areas **260b**, **260d** may be transferred through the ground plane of the circuit board **212c** to the exposed ground plane areas **270a**, **270b** that couple with the posts **230c'**, **230c**. The heat may then further be transferred through the posts **230c'**, **230c** to the housing **102** (e.g., front shell **202**) and dissipated through the exterior surface **204**.

In the example embodiment illustrated in FIG. 2C, the post **230a** is coupled directly to at least one IC (e.g., the processor **220**). In contrast, the posts **230b**, **230c**, **230c'** may be considered to be in indirect physical contact with a number of ICs through at least one or more intermediate circuit boards. For example, the post **230b** may be in indirect contact with the ADCs **240b** through circuit board **212b**. Likewise, posts **230c**, **230c'** may be considered to be in indirect physical contact with ADCs **240b**, **240d** through circuit board **212c** (and in the illustrated embodiments, also through thermal pads **250b**, **250d**).

In contrast with dissipating heat into the internal ambient air for transfer to the housing **102**, the posts **230** may provide improved conduits of thermal energy transfer and draw more of the heat generated by the processor **220** or ADCs **240b**, **240d**. This may allow for more heat to be transferred to the housing **102** (e.g., front shell **202**) for dissipation through the exterior surface **204**.

Posts **230** may generally be made of any material that provides improved thermal conductivity over ambient air. In some embodiments, one or more of the posts **230** may be made of the same metal that the front shell **202** (and the housing **102**) is made of. The posts **230** being made of the same metal may allow for there to be uniform thermal

conductivity as between the posts **230** and the housing **102**, so as to facilitate better heat transfer to the housing **102**. It may also allow the heat to be spread out evenly across all parts of the same material, so as to reduce the likelihood of concentrated hot spots at any single region of a post **230** (where such hot spots may potentially expose internal ICs to excessive heat and cause damage thereto) or on surfaces of the housing **102** (where such hot spots may cause discomfort to ultrasound operators or cause non-compliance with applicable temperature regulations).

The posts **230** may be formed in different shapes and configurations. For example, the posts **230** may be provided in a circular, square, rectangular, or other shape. Additionally or alternatively, the posts **230** may be constructed as having a solid metal interior or having a hollow interior which can then be filled with thermal paste and/or a solid block of metal. Since the metal may provide improved thermal conductivity over ambient air, a solid metal interior may provide improved heat dissipation over a configuration where there is no post **230** at all. However, to further improve heat transfer, in some embodiments, it may be possible to provide a post **230** that is hollow and filled in with thermal paste. Since thermal paste may have higher thermal conductivity over the metal of the posts **230**, the thermal paste provided within the post **230** may further improve heat transfer from the surface to which the post **230** is mated (e.g., a circuit board or an IC) towards the housing **102**. Additionally or alternatively, in some embodiments, to provide for structural integrity of a given post **230**, the hollow interior of a post **230** may be filled with a solid block of metal that is attached via an adhesive and surrounded by thermal paste.

In addition to considerations about thermal conductivity, the manufacturing process used to create the housing **102** may be taken into account when determining the shape and configuration of the posts **230**. For example, when a machining process is used to create the housing **102**, it may be suitable to perform the machining in a manner that leaves a solid metal post. However, when a die casting process is used, it may be difficult to achieve a solid metal post with the same thickness that can be obtained via the machining process. As such, when using die casting, it may be suitable to create a mold with a post having a hollow interior (with side walls having a thickness suitable for die casting), which can then be filled in the manner noted above (e.g., with thermal paste or a solid metal block).

Different methods may be used to attach the posts **230** the interior surface **206** of the front shell **202**. For example, in some embodiments, one or more of the posts **230** and the housing **102** form part of a unitary body. Such a unitary body may be created by including the posts **230** in the mold used to create the front shell **202** (e.g., if the front shell **202** is created by injection moulding and/or die casting). Additionally or alternatively, separately formed posts **230** may be attached to the front shell **202** at desired locations. For example, the front shell **202** may be formed with slots for receiving one or more of separately formed posts **230**, and such posts **230** may be attached using the slots after creation of the front shell **202**. In some embodiments, such attachment may be achieved using adhesive (e.g., Loctite™ 435). Thermal paste may also be used to enhance the thermal attachment between the separately formed posts **230** and the slots that receive the posts **230**. Referring again briefly to FIG. 2A, it can be seen that in the illustrated embodiment, post **230a** is provided as being a unitary part of the front shell **202** (shown with a hollow interior). However, post **230b** and **230c** are illustrated as separately formed posts

(also with hollow interiors) that are attached to slots receiving the posts **230b** and **230c**. This is why in the illustrated embodiments, there is a line separating the body of the posts **230b**, **230c** from corresponding slots for receiving the posts **230b**, **230c**; where such line is not present on post **230a**.

Referring to FIG. 3A, shown there generally as **300a** is an interior view of the front shell **202** shown in FIGS. 2A-2C, in accordance with at least one embodiment of the present invention. In FIG. 3A, the front shell **202** is shown only with the transducer cap **210**. The interior view of the front shell **202** provides a clear view of the interior surface **206** (as shown in FIG. 2A) of the front shell **202**. As a result, posts **230a**, **230b**, **230c**, **230c'** can be seen.

Referring to FIG. 3B, shown there generally as **300b** is a cross-sectional view of the front shell of FIG. 3A, along line A-A shown in FIG. 3A, in accordance with at least one embodiment of the present invention. In the illustrated embodiment, it can be seen that the exterior surface **204** of the front shell **202** may be configured to have a number of fins **310**. At the same time, certain regions **315** of the exterior surface **204** may be configured to have a smooth surface without any fins **310**.

The appearance of the fins **310** on an ultrasound imaging device **100** may take various forms. However, in the example embodiment illustrated in the various drawings herein (e.g., as most prominently shown in FIG. 1A), the fins may, alone or in combination with other visual elements, primarily provide a distinctive visual and decorative appearance for the ultrasound imaging device **100**. For example, the layout, arrangement, and positioning of the fins **310** may provide visual distinctiveness for the illustrated example embodiment of the ultrasound imaging device **100**.

Additionally, configuring the exterior surface **204** to have a number of fins **310** may increase the surface area of the exterior surface **204** of the front shell **202** and the housing **102** overall, so as to further improve heat dissipation. For example, the fins **310** added to the exterior surface **204** of the front shell **202** may increase the surface area of the exterior surface of the entire housing **102** by at least 30%. In one example embodiment, the fins **310** added to the front shell **204** increases the surface area of the housing **102** by 33%. As noted above, for example, in some embodiments, the total exterior surface of the housing **102** may have surface area of at least 31,525 mm² (inclusive of the grip portion **170** shown in FIG. 1A that may be covered with rubber in some embodiments).

Further, the presence of the fins **310** may provide texture on the exterior surface of the housing **102** where there may otherwise be a smooth surface. As compared to traditional wired ultrasound imaging systems where the ultrasound probe may be grasped at via an attached cable, this texture may allow a wireless ultrasound imaging device **100** to be better gripped or picked up by ultrasound operators.

Referring still to FIG. 3B, shown there are the positions of certain regions of the exterior surface **204** of the front shell **202** relative to the post **230a**, **230b** on the interior surface **206** of the front shell **202**. For example, as shown, the smooth region **315** of the exterior surface **204** may be provided opposite the post **230b**. Additionally, it may be possible to position the fins **310** on a region of the exterior surface **204** opposite a location on the interior surface **206** that is directly coupled to the post **230a**. Configuring the fins **310** to be directly opposite a post **230a** may allow heat to be transferred more easily from the post **230a** towards a region of the exterior surface **204** having increased surface area, so that the heat can be more easily dissipated therefrom. At the same time, the increased surfaced area created by the fins

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310 may spread the heat channeled by the post **230a** over a larger surface area and reduce the likelihood of significant hot spots being created on the exterior surface **204** at regions directly opposite the area where the post **230a** is coupled. This effect of spreading the heat over a larger area may be further enhanced by having the finned region of the exterior surface **204** be larger in size than the area on the interior surface **206** that is directly coupled to the post **230a**. Additionally, the finned region may increase the distance (e.g., create a small gap) between the surface immediately opposite where a post **230a** is coupled and the surface that comes into contact with the ultrasound operator. This small air gap may reduce the heat sensation felt by the ultrasound operator.

Referring to FIG. 4A, shown there generally as **400a** is a rear view of a partially-assembled ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention. FIG. 4A generally shows an interior view of when the components of FIGS. 2A-2C are assembled. From the illustrated rear view, the front shell **202**, transducer cap **210**, and circuit boards **212c**, **212d** can be seen.

Referring to FIG. 4B, shown there generally as **400b** is a cross-sectional view of the partially-assembled ultrasound imaging device shown in FIG. 4A along the line B-B, in accordance with at least one embodiment of the present invention. Referring briefly also to FIG. 3A, it can be seen that the section line B-B may generally cut through portions of posts **230a** and **230b**. FIG. 4B provides a view similar to that shown in FIG. 3B, except a number of additional components shown in FIGS. 2A-2C are also shown.

In FIG. 4B, it can be seen that posts **230a**, **230b** are directly coupled to the interior surface **206** of the front shell **202**. Circuit board **212a** can be seen to be fitting around the posts **230a**, **230b**, and processor **220** provided on circuit board **212c** is mated directly to the post **230a**. Post **230b** is mated to an upper region of the surface of circuit board **212b** that faces the front of the ultrasound imaging device **100**. Also, the ADCs **240** provided on boards **212b**, **212d** are mated to circuit board **212c** via thermal pads **250**. As discussed above, the thermal pads **250** may be mated to the ground plane of the circuit board **212c**, which is then indirectly mated to additional posts **230c**, **230c'** (not shown in FIG. 4B) through the ground plane of the circuit board **212c** for heat transfer. FIG. 4B also shows the coupling of the transducer array **208** to circuit board **212c**, and the transducer cap **210**.

Also viewable in FIG. 4B are a number of metallic spacers **405** (not shown in earlier figures) which may allow the circuit boards **212d**, **212c**, **212b**, **212a** to be held together. In such embodiments, the circuit boards **212** may be provided with mounting holes (not shown) which are connected to the ground planes of the various circuit boards (including circuit board **212c**). Metallic screws (not shown in FIG. 4B) may then be used to thread through the metallic spacers **405** and secure the circuit boards **212d**, **212c**, **212b**, **212a** together. One or more of the circuit boards **212d**, **212c**, **212b**, **212a** may then be secured to the housing **102** (e.g., to the front shell **202** and/or the rear shell **502**) through the same or additional mounting holes provided on the circuit boards **212d**, **212c**, **212b**, **212a**, also using metallic screws. The metallic screws travelling through multiple circuit boards **212** and metallic spacers **405** and eventually having indirect contact with the housing **102** may provide an additional heat transfer path from various ICs provided on the circuit boards **212d**, **212c**, **212b**, **212a** to the housing **102**, and thereby further improve heat dissipation. In various

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embodiments, the metallic spacers **405** may be any form of suitable metallic component that allows for heat transfer. For example, the metallic spacer **405** may be a bushing or a bolt, and either threaded or unthreaded.

In some embodiments, the circuit boards **212d**, **212c**, **212b**, **212a** may be configured to have exposed ground planes in areas where the circuit boards come into contact with the metallic spacers **405**. Such a configuration may enhance heat transfer amongst the multiple circuit boards **212d**, **212c**, **212b**, **212a** through the metallic spacers **405**, and specifically, enhance heat transfer towards the ground plane of circuit board **212c**. As discussed above in relation to FIG. 2C, the ground plane of **212c** is coupled to posts **230c**, **230c'** provided on the front shell **202** of the housing **102**, so that heat can be dissipated therefrom. As illustrated in FIG. 4B, the metal spacers **405** are shown in the cross-sectional view along line B-B of FIG. 4A. However, the metal spacers **405** and corresponding mounting holes may be provided at any area of one or more of the circuit boards **212d**, **212c**, **212b**, **212a** that allows a common screw or other mechanism to bind the one or more of the circuit boards **212d**, **212c**, **212b**, **212a** together and/or to the housing **102**.

Additionally, there may be a number of connectors (not shown) that allow one or more of the various circuit boards **212d**, **212c**, **212b**, **212a** to be coupled together for electrical communication. These various connectors may have metallic ground pins that may provide a further heat transfer mechanism amongst the ground planes of the circuit boards **212d**, **212c**, **212b**, **212a**, and allow heat to be channeled towards the ground plane of circuit board **212c** which is physically coupled to posts **230c**, **230c'**.

As mentioned above, to provide ultrasound images with high quality and desired tissue penetration, the ultrasound image device **100** may be provided with a number of ADCs **240b**, **240d**, and a processor **220** that is capable of carrying heavy loads when performing image processing. For example, in some embodiments, the ADCs **240b**, **240d**, processor **220**, and/or other ICs may collectively or individually consume at least 3 watts of power (e.g., while imaging or in any other active mode). In one example embodiment, a programmable System on a Chip (SoC) may be used and such IC may consume 3.5-4.5 watts of power while imaging. This level of power consumption may be considered to be relatively high for portable wireless devices; and the present embodiments may be particularly applicable in such situations to dissipate the higher levels of heat generated by the increased power consumption.

While the embodiments described herein may be employed in any context where heat is generated from ICs within the housing **102**, the techniques discussed may be particularly applicable in embodiments where it is desired to dissipate heat generated from general purpose ICs. Unlike application-specific integrated circuits (ASICs) which can be designed to perform within particular heat parameters while still carrying heavy loads, general purpose ICs may not be designed in such a manner and, as a result, may generate more heat. However, use of general-purpose ICs allows ultrasound imaging devices **100** to be designed and constructed in a more straightforward and cost-effective manner. As such, the techniques described herein may facilitate heat dissipation using general-purpose ICs without resorting to the expense and effort of designing a dedicated ASIC that outputs lower heat. Indeed, the improved heat dissipation mechanisms discussed herein may reduce the possibility of IC failures and/or the surface temperature of the housing **102** being non-compliant with applicable safety

regulations (for ultrasound imaging devices **100** generally, and in particular embodiments where general-purpose ICs are used).

Referring to FIG. 5A, shown there generally as **500a** is an exterior view of the rear shell **502** that forms part of the housing **102** of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention. To provide substantially uniform thermal conductive properties across the entire housing **102**, in some embodiments, the rear shell **502** may also be made of the same metal as the front shell **202**. As shown, the rear shell **502** may have an exterior surface **204'** that includes a slot **510** for receiving the removable battery **106** (not shown in FIG. 5B, but shown included in the view of FIG. 1B). The rear shell **502** may provide a latch **512** for securing the battery **106** in place when it is placed within the slot **510**. It will be understood by persons skilled in the art that a latch **512** is simply one way of securing the battery **106** in place when it is in the slot **510**, and that other mechanisms may be possible. Moreover, in some embodiments, the ultrasound imaging device **100** may not have a removable battery, and instead, an internal battery may be provided.

Referring to FIG. 5B, shown there generally as **500b** is an interior view of the rear shell **502** that forms part of the housing **102** of the ultrasound imaging device of FIGS. 1A-1D, in accordance with at least one embodiment of the present invention. The rear shell **502** may have an interior surface **206'** which is placed adjacent the circuit boards **212d**, **212c** shown in FIG. 4A when the rear shell **502** mates with the front shell **202** and the ultrasound imaging device **100** is in assembled form. Referring briefly also to FIG. 4B, the circuit boards **212a**, **212b**, **212c**, **212d** may be secured together (e.g., via, or as separated by, metallic spacers **405**) to form a circuit board assembly. The circuit board assembly may then be secured to the rear shell **502** (and housing **102**) to allow for an additional heat transfer path from the ICs to the housing **102**. In some embodiments, the metallic screws that secure the circuit board assembly together may also be used to secure the circuit boards to the housing **102**. In some embodiments, there may be one set of screws that binds the circuit boards **212d**, **212c**, **212b**, **212a** together, and another set of screws that bind the bounded circuit board assembly to the housing **102**. As shown in FIG. 5B, there are a number of mounting holes **530** that may be used to receive metallic screws so as to allow for the circuit board assembly to be secured to the rear shell **502**.

Referring simultaneously to FIG. 1C, FIG. 4B, and FIG. 5A, it can be seen that when the ultrasound imaging device **100** is in assembled form, the battery **106** (as shown in FIG. 1C) that powers the ultrasound imaging device **100** is positioned on a side of the ultrasound imaging device **100** that is opposite the fins **310**. Since the battery **106** is typically made of a material that is less thermally conductive than the metallic surface **204'** (as shown in FIG. 5A) of the housing **102**, it may be difficult for heat to travel through the battery **106** to dissipate from the exterior surface **204'** of the rear shell **502**. The heat generated by the internal components of the ultrasound imaging device **100** may thus generally be channeled to the front shell **202** (as shown in FIG. 1C) for dissipation. The positioning of the posts **230** to couple directly with the interior surface **206** of the front shell **202** (as shown in FIG. 4B) may thus assist with such channeling of heat. In addition, the placement of fins **310** on an area of the exterior surface of the housing **102** opposite the side of the ultrasound imaging device **100** where the battery **106** is positioned may provide a greater surface area

for dissipating the additional heat that would not be able to be channeled towards the rear shell **502** due to the battery **106**.

Referring to FIG. 6A, shown there generally as **600a** is an exterior perspective exploded view of the rear shell **502** shown in FIGS. 5A-5B, in accordance with at least one embodiment of the present invention. As discussed above in relation to FIG. 1C, the rear shell may have recesses on its sides to allow for placement of antennas for wireless communications. While a housing **102** that is made substantially of metal may improve heat dissipation, metal is generally a ferromagnetic material that may interfere with proper operation of antennas if the antennas are placed within the metal housing **102**. The recesses may thus allow the housing **102** to be made substantially of metal (and achieve as much heat dissipation as possible), but also provide a mechanism for placement of the antennas on the exterior of the housing **102** so that wireless communications may not be unduly impeded.

As compared to some mobile communication devices (e.g., mobile phones) that have metallic backings, a larger portion of the housing **102** of the ultrasound imaging device **100** may be made of metal. For example, in the illustrated embodiments, the entire housing **102** (except for the transducer cap **210**) may be made of metal. Whereas a traditional mobile communications device may typically have a screen or other gaps in their housing that would allow wireless signals to be effectively transmitted from an antenna positioned within a metal housing, the mobile wireless ultrasound device **100** of the present embodiments does not have a screen or such gaps. Instead, a larger portion of the housing **102** may be constructed of metal to better facilitate dissipation of the higher level of heat generated by the higher wattage processing components (e.g., ADCs **240b**, **240d**) in an ultrasound imaging device **100**.

In the illustrated embodiment of FIG. 6A, there may be antennas **602a**, **602b**, which are to be placed within recesses on the two sides of rear shell **502**. To provide improved operation of the antennas **602a**, **602b**, there may also be provided shims **604a**, **604b** to space the respective antenna **602a**, **602b** away from the metallic rear shell **502**. In various embodiments, the antennas **602a**, **602b** may provide wireless communications on various frequencies (e.g., 2.4 Ghz or 5 Ghz) that are suitable to enable communications using any wireless communication protocols (including Wi-Fi™ or Bluetooth™). In various embodiments, a single antenna **602a** may be a wireless antenna module that includes multiple types of antennas that communicate on multiple frequencies and/or protocols (e.g., the module may include both Wi-Fi™ and Bluetooth™ antennas). In such embodiments, the same antenna module may be added in both the left and right recesses of the rear shell **502** to allow for improved radio link performance using multiple-in and multiple-output (MIMO) methods. The shape of the recess may be configured to fit any type of suitable antenna module that allows for desired wireless communications. For example, in one example embodiment, the antenna module 001-0021, manufactured by LSR™ may be used.

Referring still to FIG. 6A, covers **108a**, **108b** may be placed over the antennas **602a**, **602b** so as to form substantially flat side surfaces of the ultrasound imaging device **100**. The covers **108a**, **108b** may generally be made of non-ferromagnetic material so as to not interfere with the operation of the antennas **602a**, **602b**. In some embodiments, the covers **108a**, **108b** may form a seal with the adjacent exterior surfaces of the housing **102** so as to prevent ingress (e.g., from liquid or dust). In embodiments where the slot **510** for

the battery 106 is constructed to also be sealed when the battery 106 is in place, the entire ultrasound imaging device 100 may be considered to be protected from ingress into the interior of the device 100. In some embodiments, the housing may have an International Protection Marking (IP Code) ingress rating of at least IPX7.

As shown in FIG. 6A, each of the antennas 602a, 602b may have corresponding connector wires 610a, 610b for connecting to and communicating with the electronic components inside the housing 102. To allow for the connector wires 610a, 610b to electronically couple with internal electronic components, the rear shell 502 may provide small openings in the recesses where the antennas 602a, 602b are to be placed. The connector wires 610a, 610b may then be threaded through these openings to the interior of the housing 102 so that they may, for example, connect with circuit boards 212a, 212b, 212c, 212d (as shown in earlier figures) and other ICs provided thereon.

As discussed above, it may be possible to use the same antenna modules (having both Wi-Fi™ and Bluetooth™ antennas) in each of the left and right recesses provided on the rear shell 502. However, if the same antenna module is used, the connector wires 610a, 610b may not always be positioned towards the same surface of the rear shell 502 when placed within the recesses. For example, in the view and orientation shown in FIG. 6A, the connector wire 610a is shown as being provided on the top right corner of the antenna module 602a. To allow for this connector wire 610a to thread into the interior of the housing 102, an opening 620a may be provided in the corresponding corner of the recess. As shown in FIG. 6A, the opening may be provided on a corner of the recess that is proximate the interior surface of the rear shell 502. In contrast, if the same antenna module is placed in the opposite recess provided on the rear shell 502, the connector wire 610b provided with the antenna module 602b may be flipped along its lengthwise axis, so that connector wire 610b extends from the upper left hand corner of the antenna module 602b. The connector wire 610b may then be oriented towards the exterior surface of the rear shell 502 instead of the interior surface of the rear shell 502. In some embodiments, an opening 620b may be provided in the corresponding corner of that recess, which is proximate the exterior surface of the housing 102. This opening 620b may be more clearly viewable in FIG. 6B.

Referring simultaneously to FIG. 6B, shown there generally as 600b is an interior perspective exploded view of the rear shell shown in FIGS. 5A-5B, in accordance with at least one embodiment of the present invention. The view 600b shows the same components of FIG. 6A, but flipped along the longest axis of the rear shell 502. The antenna 602a, shim 604a, and cover 108a are illustrated. As shown, a corresponding end 620a' of the opening 620a (as shown in FIG. 6A) may be provided on the interior surface of the rear shell 502, so as to allow the connector wire 610a to protrude into the interior surface of the housing 102.

FIG. 6B also shows the antenna 602b, shim 604b, and cover 108b that may be placed in the opposite recess of the rear shell 502. As shown, the opening 620b may be provided near a corner of the recess that is proximate the exterior surface of the rear shell 502, so as to align with the positioning of the connector wire 610b on the antenna 602b. The opening 620b may tunnel through the body of the rear shell 502 to its corresponding end 620b' (e.g., through the depth of the shortest axis of the rear shell 502) so as to allow the connector wire 610b to be presented to the interior surface of the housing 102. This tunneling may not be required for the opening 620a because the opening 620a is

provided on a corner of the recess that is already adjacent the interior surface of the rear shell 502.

Referring to FIG. 7, shown there generally as 700 is an interior perspective view of a partially-assembled configuration of the components shown in FIGS. 6A-6B, in accordance with at least one embodiment of the present invention. FIG. 7 shows the antenna 602b being provided within in the right-hand recess of the rear shell 502. In assembled form, the connector wire 610b of the antenna 602b may be inserted in opening 620b (not shown in FIG. 7) provided near the exterior surface of the rear shell 502, so as to tunnel through the body of the rear shell 502 and protrude through the opposite end 620b' of the opening 620b. Also viewable in FIG. 7 is the connector wire 610a of antenna 602a (shown in FIGS. 6A and 6B) that protrudes through opening 620a (as shown in FIG. 6A) and exits at the opposite end 620a' on the interior surface of the rear shell 502. Also viewable in FIG. 7 are the covers 108a, 108b which may be placed over the recesses, and mounting holes 530 to which circuit boards 212 may be mounted, as discussed above.

Interpretation of Terms

Unless the context clearly requires otherwise, throughout the description and the claims:

“comprise”, “comprising”, and the like are to be construed in an inclusive sense, as opposed to an exclusive or exhaustive sense; that is to say, in the sense of “including, but not limited to”;

“connected”, “coupled”, or any variant thereof, means any connection or coupling, either direct or indirect, between two or more elements; the coupling or connection between the elements can be physical, logical, or a combination thereof;

“herein”, “above”, “below”, and words of similar import, when used to describe this specification, shall refer to this specification as a whole, and not to any particular portions of this specification;

“or”, in reference to a list of two or more items, covers all of the following interpretations of the word: any of the items in the list, all of the items in the list, and any combination of the items in the list;

the singular forms “a”, “an”, and “the” also include the meaning of any appropriate plural forms.

Unless the context clearly requires otherwise, throughout the description and the claims:

Words that indicate directions such as “vertical”, “transverse”, “horizontal”, “upward”, “downward”, “forward”, “backward”, “inward”, “outward”, “vertical”, “transverse”, “left”, “right”, “front”, “back”, “top”, “bottom”, “below”, “above”, “under”, and the like, used in this description and any accompanying claims (where present), depend on the specific orientation of the apparatus described and illustrated. The subject matter described herein may assume various alternative orientations. Accordingly, these directional terms are not strictly defined and should not be interpreted narrowly.

Where a component (e.g. a software module, processor, assembly, device, circuit, etc.) is referred to above, unless otherwise indicated, reference to that component (including a reference to a “means”) should be interpreted as including as equivalents of that component any component which performs the function of the described component (i.e., that is functionally equivalent), including components which are not structurally equivalent to the disclosed structure which performs the function in the illustrated exemplary embodiments of the invention.

Specific examples of systems, methods and apparatus have been described herein for purposes of illustration. These are only examples. The technology provided herein can be applied to systems other than the example systems described above. Many alterations, modifications, additions, omissions, and permutations are possible within the practice of this invention. This invention includes variations on described embodiments that would be apparent to the skilled addressee, including variations obtained by: replacing features, elements and/or acts with equivalent features, elements and/or acts; mixing and matching of features, elements and/or acts from different embodiments; combining features, elements and/or acts from embodiments as described herein with features, elements and/or acts of other technology; and/or omitting combining features, elements and/or acts from described embodiments.

It is therefore intended that the following appended claims and claims hereafter introduced are interpreted to include all such alterations, modifications, permutations, additions, omissions, and sub-combinations as may reasonably be inferred. The scope of the claims should not be limited by the preferred embodiments set forth in the examples, but should be given the broadest interpretation consistent with the description as a whole.

What is claimed is:

1. A wireless ultrasound imaging apparatus, comprising: a body with an imaging end, a non-imaging end, and a side surface between the imaging end and the non-imaging end, the side surface being holdable during operation of the ultrasound imaging apparatus; a transducer array positioned at the imaging end of the body; at least one integrated circuit (IC) operatively connected to the transducer array; and an antenna operatively connected to the at least one IC, the antenna for providing wireless communication of ultrasound image data; wherein the body comprises a metallic housing, the metallic housing enclosing the transducer array and the at least one IC, and wherein the metallic housing comprises an interior surface opposite the holdable side surface of the body; wherein during imaging, power is consumed by the at least one IC, to generate ultrasound image data for wireless transmission via the antenna; and wherein a post is disposed between the at least one IC and the interior surface that is opposite the holdable side surface of the body, the post being coupled directly to the interior surface of the metallic housing so that heat, generated as a result of the consumption of power by the at least one IC during imaging, is transferred via the post to the metallic housing and dissipated.
2. The wireless ultrasound imaging apparatus of claim 1, wherein the metallic housing comprises a material having a thermal conductivity of between 55 to 167 watts per meter kelvin (W/(m·K)) and a density of between 1.77 to 5 grams per cubic centimeter (g/cm³).
3. The wireless ultrasound imaging apparatus of claim 2, wherein the material comprises an aluminum alloy.
4. The wireless ultrasound imaging apparatus of claim 2, wherein the material comprises a magnesium alloy.
5. The wireless ultrasound imaging apparatus of claim 1, wherein the power consumed by the at least one IC is between 3 to 4.5 watts of power.
6. The wireless ultrasound imaging apparatus of claim 1, wherein the metallic housing comprises a grip portion and a non-grip portion, and the grip portion is covered with an

insulating polymer-based material, and the non-grip portion is uncovered such that the holdable side surface of the metallic housing is exposed at the non-grip portion.

7. The wireless ultrasound imaging apparatus of claim 1, wherein the holdable side surface of the metallic housing forms the outermost surface of the wireless ultrasound imaging apparatus, and the holdable side surface comprises a recess for placement of the antenna.

8. The wireless ultrasound imaging apparatus of claim 7, wherein a shim is positioned in the recess between the metallic housing and the antenna to space the antenna away from the metallic housing.

9. The wireless ultrasound imaging apparatus of claim 7, wherein a non-ferromagnetic cover is placed over the antenna, and wherein the non-ferromagnetic cover forms a seal with an adjacent exterior surface of the metallic housing to prevent ingress into the interior of the wireless ultrasound imaging apparatus.

10. The wireless ultrasound imaging apparatus of claim 1, wherein the at least one IC comprises an Analog to Digital Converter (ADC) and a graphic processor.

11. The wireless ultrasound imaging apparatus of claim 1, wherein the at least one IC comprises a programmable System on a Chip (SoC).

12. The wireless ultrasound imaging apparatus of claim 1, wherein the metallic housing comprises a front shell and a rear shell, and at least one of the front shell or the rear shell is formed to receive a removable battery.

13. The wireless ultrasound imaging apparatus of claim 1, wherein the metallic housing comprises a slot for receiving a removable battery.

14. The wireless ultrasound imaging apparatus of claim 13, wherein the wireless ultrasound imaging apparatus is sealed when the removable battery is positioned in the slot, and the wireless ultrasound imaging apparatus with the removable battery in place is protected from ingress into the interior of the wireless ultrasound imaging apparatus.

15. A method of facilitating dissipation of heat in a wireless ultrasound imaging apparatus, the method comprising:

- providing a body for the wireless ultrasound imaging apparatus, the body comprising an imaging end, a non-imaging end, and a side surface between the imaging end and the non-imaging end, with the side surface being holdable during operation of the ultrasound imaging apparatus, the body comprising a metallic housing enclosing a transducer array positioned at the imaging end of the body and at least one integrated circuit (IC) operatively connected to: the transducer array and an antenna, the antenna for providing wireless communication of ultrasound image data, wherein the metallic housing comprises an interior surface opposite the holdable side surface of the body; and activating the at least one IC during operation of the wireless ultrasound imaging apparatus, wherein power is consumed by the activated at least one IC to generate ultrasound image data for wireless transmission via the antenna, and wherein heat generated as a result of the consumption of power by the at least one IC during imaging is transferred to the metallic housing and dissipated therefrom via at least one post that is disposed between the at least one IC and the interior surface of the metallic housing that is opposite the holdable side surface of the body, the post being coupled directly to the interior surface of the metallic housing.

16. The method of claim 15, wherein the metallic housing comprises a material having a thermal conductivity of between 55 to 167 watts per meter kelvin (W/(m·K)) and a density of between 1.77 to 5 grams per cubic centimeter (g/cm³). 5

17. The method of claim 15, wherein the power consumed by the at least one IC is between 3 to 4.5 watts of power.

18. The method of claim 15, wherein the metallic housing comprises a front shell and a rear shell, and at least one of the front shell or the rear shell is formed to receive a 10 removable battery.

19. The method of claim 15, wherein the metallic housing comprises a slot for receiving a removable battery.

20. The method of claim 19, wherein the wireless ultrasound imaging apparatus is sealed when the removable 15 battery is positioned in the slot, and the wireless ultrasound imaging apparatus, with the battery in place, is protected from ingress into the interior of the wireless ultrasound imaging apparatus.

21. The method of claim 15, wherein the holdable side 20 surface of the metallic housing that forms the outermost surface of the wireless ultrasound imaging apparatus, and the holdable side surface comprises a recess for placement of the antenna.

22. The method of claim 21, wherein a non-ferromagnetic 25 cover is placed over the antenna, and wherein the non-ferromagnetic cover forms a seal with an adjacent exterior surface of the metallic housing to prevent ingress into the interior of the wireless ultrasound imaging apparatus.

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