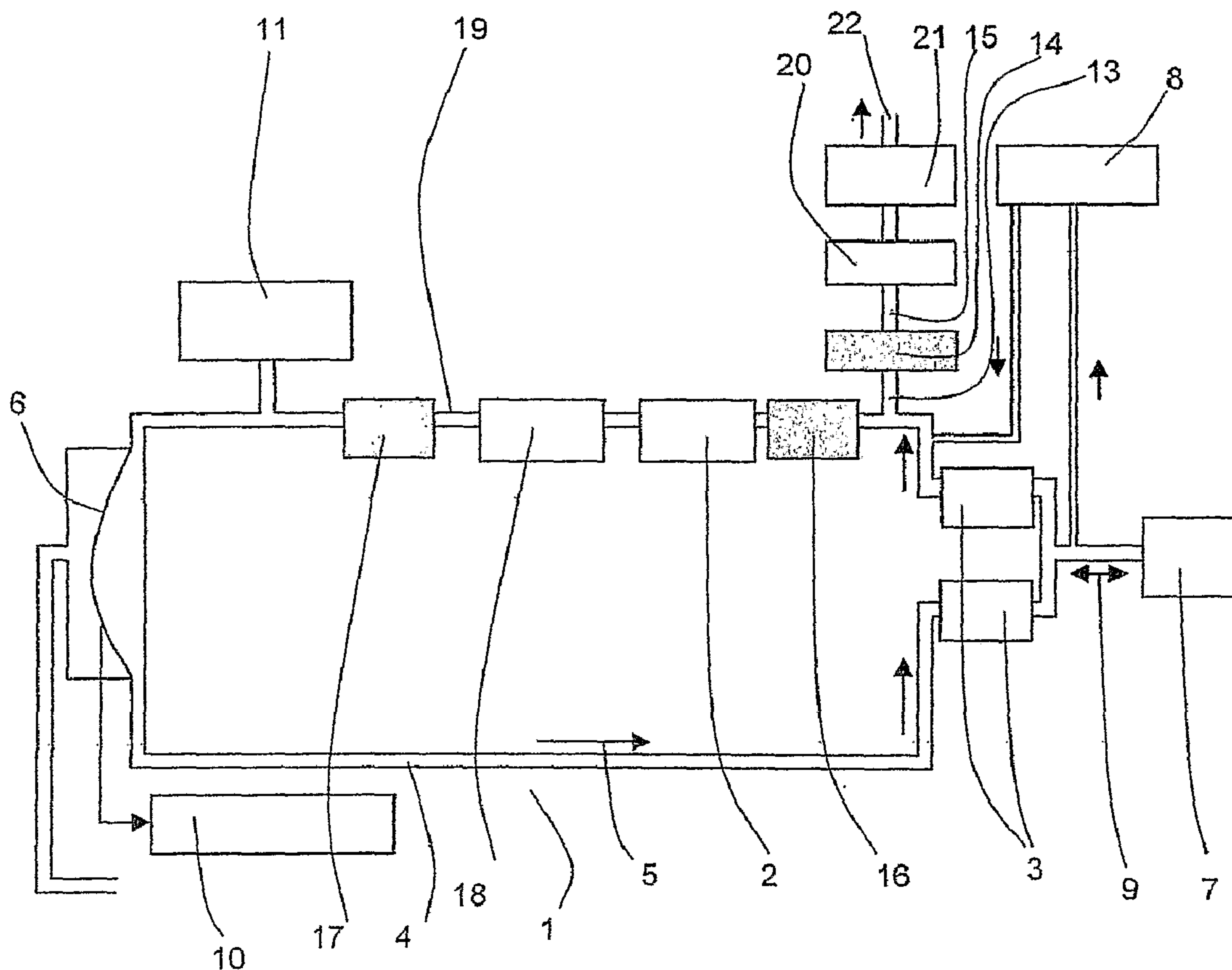




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(72) **Inventeurs/Inventors:**
BORM, PIETER, NL;
WESTERKAMP, BART, NL
(73) **Propriétaire/Owner:**
LOWENSTEIN MEDICAL TECHNOLOGY S.A., LU
(74) **Agent:** OSLER, HOSKIN & HARCOURT LLP

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(57) **Abrégé/Abstract:**

Method and apparatus for respirating patients, with means for circulating gas in a conduit system, for varying the pressure in the line system, for measuring the gas flow, with connecting means for the patient and supplies for the components of the gas and for



(57) Abrégé(suite)/Abstract(continued):

withdrawing carbon dioxide, with a first closing device to a discharge line of breathing gas, with in the line system, behind the connecting means to the discharge line a second closing means, and behind that and at a distance there from a third closing means, whilst means are provided by means of which the second and third closing means can be controlled such, that the part of the line system between the second and the third closing means can be closed off, whilst the line system further is provided with means for the generating of a gas flow.

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(72) Inventors; and

(75) Inventors/Applicants (for US only): **BORM, Pieter** [NL/NL]; Normandiëlaan 77, NL-5627 HP Eindhoven (NL). **WESTERKAMP, Bart** [NL/NL]; Klipperstraat 28, NL-1826 DW Alkmaar (NL).(74) Agent: **KOOMEN, Melanie, J., I.**; Kennenmerstraatweg 35, NL-1814 GB Alkmaar (GB).

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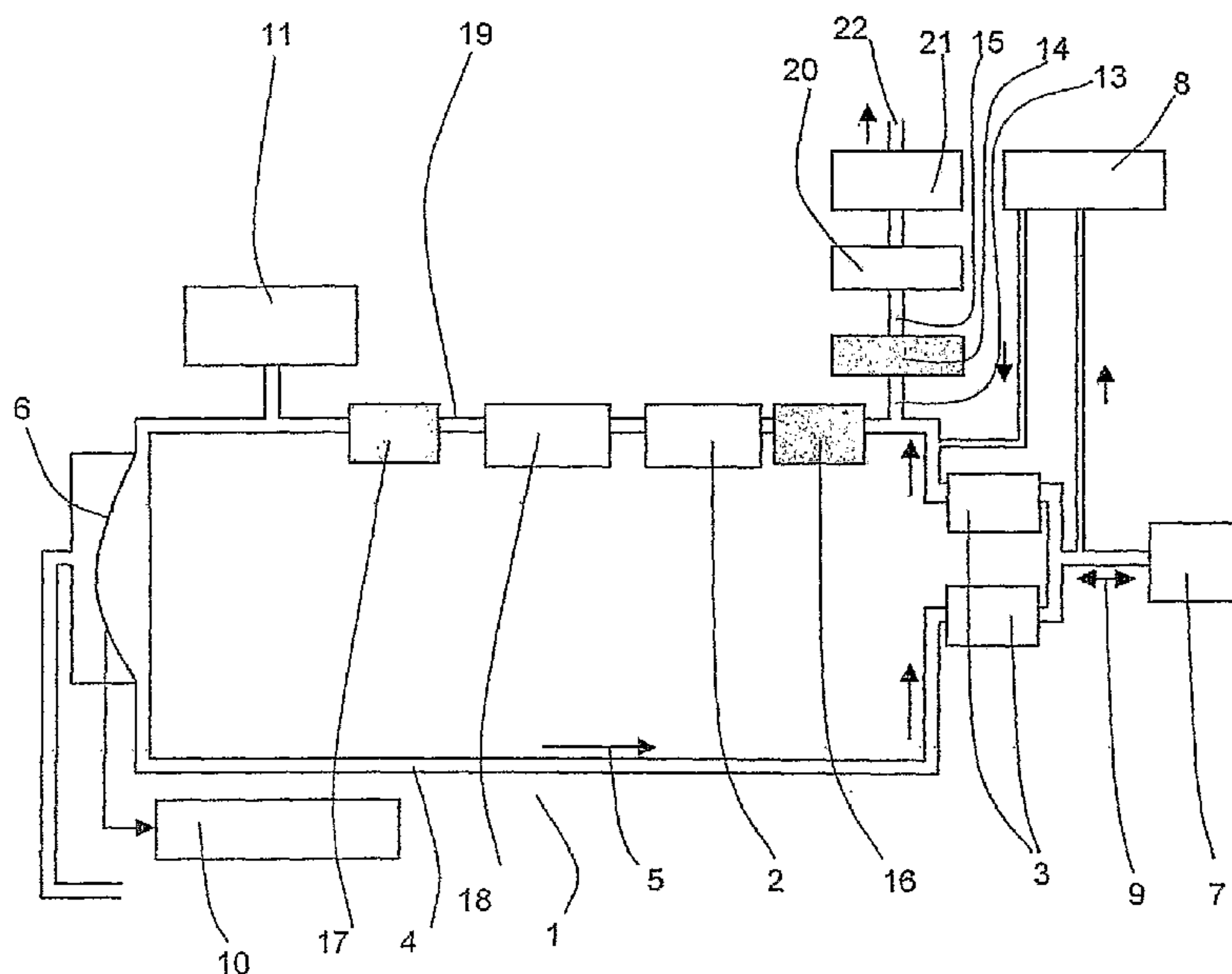


FIG. 1

(57) Abstract: Method and apparatus for respirating patients, with means for circulating gas in a conduit system, for varying the pressure in the line system, for measuring the gas flow, with connecting means for the patient and supplies for the components of the gas and for withdrawing carbon dioxide, with a first closing device to a discharge line of breathing gas, with in the line system, behind the connecting means to the discharge line a second closing means, and behind that and at a distance there from a third closing means, whilst means are provided by means of which the second and third closing means can be controlled such, that the part of the line system between the second and the third closing means can be closed off, whilst the line system further is provided with means for the generating of a gas flow.

Method and apparatus for respirating patients.

The present invention relates to a method for respirating of patients, whereby use is made of an apparatus which is provided with means for circulating a gas in one direction in a line or conduit system, with means for varying the pressure in the line system in accordance with a certain respirating pattern, with means for measuring the flow of the gas and the composition of the gas, whilst the line system is provided with connecting means for the patient and with one or more supplies for the various components of the respiratory gas, whereby the line system further is provided with a connecting means to a discharge line that is provided with a closing device for the discharge out of the line system of gas, whilst in the line system, as seen in the direction of the circulation of the gas, behind the connecting means to the discharge line a second closing means is provided.

Such a method is known.

With the known method it is possible to switch from an open system, in which the patient again and again breathes in fresh breathing gas and the breathing gas exhaled by the patient is discharged completely out of the line system (non-rebreathing), to a half closed system, in which a part of the breathing gas exhaled by the patient is circulated once again and a part is discharged outside (some form of rebreathing).

The known method in the closed system has the drawback, that the "washing in" of the patient, that is to say the intake of anesthetic gas by the patient, takes a relatively long time. The patient among other things has nitrogen in his lungs, which has to be removed before the anesthetic can be started. To that end the patient is administered 100% oxygen until practically all nitrogen has been ventilated out of the lungs (the "washing" of the lungs with oxygen). In the closed system this takes much time, because each time the oxygen is inhaled together with a part of the gas that is already present. After the washing of the lungs of the patient with oxygen an anesthetic gas, here the carrier gas, such as xenon, is supplied, of which the patient takes in and exhales again a part. The amount of oxygen and xenon that is taken in is each time compensated with only xenon until the desired concentration of oxygen and the desired concentration of xenon is obtained in the breathing gas, which is the

case only after a long time. The anesthetic or sedation here has to take place by other means.

5 In the half closed system a surplus of xenon, together with oxygen or not, is allowed to flow into the line system, by which the system gets to be overfilled. This is compensated by a "pop-off" system, in which a part of the gas in the system is discharged outside. Because of this the concentration of xenon increases. The more gas is supplied the faster the patient is washed in. This however leads to a substantial loss of gas.

10

It is an object of the invention to obviate this drawback of the known method.

The method according to the invention to that end is characterized in that, as seen in the direction of circulation of the breathing gas, behind the second closing means and at a distance therefrom a third closing means is provided, in which the method comprises the following steps:

15 Opening of the first closing means, opening of the second and third closing means, feeding into the line system of a first gas, closing of the second and third closing means, feeding into the line system of the first gas, varying of the pressure in the line system in accordance with a certain respirating pattern for supplying to the patient of the first gas, feeding into the line system of a second gas, determining the arrival of the second gas at the mouth of the patient, closing of the first closing means and the opening of the second and third closing means or the opening of the second and third closing means and closing of the first closing means and the circulating in the system of the first and second gas.

25

According to a characteristic of the method according to the invention the first gas consists of oxygen or a mixture of oxygen and another gas.

30 According to a further characteristic of the method according to the invention the second gas consists of an elementary gas, such as for instance xenon, helium, argon or a composite gas, for instance laughing gas, or a mixture of a gas or gases with a vapour anesthetic.

According to a further characteristic of the method according to the invention the gas is circulated in the line system in such a way, that the duration of one circulation of the gas is 10 seconds at the most, more in particular 5 seconds at the most, more in particular 3 seconds at the most, and even more in particular 2,5 seconds at the most.

The invention further relates to an apparatus for the application of the method, which apparatus is provided with means for the circulating in one direction in a line or conduit system of a breathing gas, an anesthetic gas or a therapeutic gas, with means for varying the pressure in the line system in accordance with a certain respirating pattern, with means for measuring the flow of the gas and the composition of the gas, whilst the line system is provided with connecting means for the patient and with one or more supply lines for the various components of the respiratory gas and with means for withdrawing of the carbon dioxide exhaled by the patient in the line system, whereby the line system further is provided with a connecting means to a discharge line that is provided with a first closing device for the discharge out of the line system of breathing gas, whilst in the line system, as seen in the direction of the circulation of the gas, behind the connecting means to the discharge line a second closing means is provided, characterized in that, as seen in the direction of circulation of the breathing gas, behind the second closing means a third closing means is provided, whilst means are provided by means of which the second and third closing means can be controlled in such a way, that the section of the line system situated between the second closing means and the third closing means can be closed off, whilst the line system further is provided with means for the generating of a gas flow.

According to a characteristic of the apparatus according to the invention the capacity of the means for the generating of a gas flow is adapted to the volume of the line system in such a way, that the duration of one circulation of the gas is 10 seconds at the most, more in particular 5 seconds at the most, more in particular 3 seconds at the most, and even more in particular 2,5 seconds at the most.

According to a further characteristic of the apparatus according to the invention the means for the generating in the line system of a gas flow consist of a circulation blower.

5 According to another characteristic of the apparatus according to the invention the means for the generating in the line system of a gas flow are provided in the part of the line system that, as seen in the direction of the flow of the breathing gas, is situated behind the second closing means, and these are more in particular provided in the part of the line system that is situated between the second closing means and
10 the third closing means.

With the method and apparatus according to the invention it is possible to wash in a patient in a quick and safe manner with the occurrence of no or only little loss of expensive gases.

15

Further characteristics and particulars of the method and apparatus according to the invention will be described with reference to the drawing of an example of an embodiment.

20 In the example of an embodiment shown in the drawing the apparatus 1 is provided with means, among which the device 11 for the supplying of the various components of the respiratory gas, anesthetic gas or therapeutic gas, with means for circulating in one direction 5 in a closed line or conduit system 4 of respiratory gas, anesthetic gas or therapeutic gas, and with means 6 for varying the pressure in the line system
25 4 in accordance with a certain respirating pattern to allow the ventilation of the patient 7. Further in the line system 4 at the connecting means for the patient 7 means are provided, such as the apparatus 8, for the determination of the composition of the gas breathed in and the gas breathed out 9 by the patient. In the drawing is shown the principle of sampling removal. If so desired the gas that has been
30 removed can be fed back into the system. It is also possible to make use of a measuring system directly in the gas breathed in and the gas breathed out 9. In the closed system by means of the sensor 10 the volume or the flow of the respiration by the patient can be measured, during spontaneous ventilation as well as during breathing upon the patient or in a given case supportive breathing upon the patient.

In the example of an embodiment shown the sensor 10 is provided in the part of the line system 4 that, as seen in the direction of circulation of the breathing gas, is situated behind the means 6 for varying the pressure in the line system.

5 The apparatus 11 provides the supply of the gases and the vaporous anesthetics into the system.

The line system 4 is provided with a connection 13 to a discharge line 15 provided with a first closing means, such as a first valve 14, for the discharge out of the line system 4 of respiratory gas.

10 In the line system 4, as seen in the direction of the circulation 5 of the gas, behind the connecting means 13 to the discharge line 15, a second closing means or second valve 16 is provided. Behind the second valve 16 in this example of an embodiment a circulation blower 18 and a carbon dioxide absorber 2 are provided. Behind this, as seen in the direction of circulation 5 of the breathing gas, a third closing means or third valve 17 is provided. The second valve 16 and the third valve 17 can be
15 controlled in such a way, that the part 19 of the line system 4 situated therein between can be closed off from the circulation of the respiratory gas, and in this manner forms a closed off section in which a particular gas can be stored.

20 When the first valve 14 is closed no gas can escape the line system through the discharge line 15. When the valves 16 and 17 are open the breathing gas can flow freely to circulate in the line system. The system functions as a completely closed system.

25 When the first valve is 14 opened gas can be discharged through the discharge line 15 and the outlet 22 of the discharge line 15 out of the line system 4. Valve 16 and 17 are opened. The system functions as a half closed system. In the line system 4 the composition of the gas is measured (not shown in the drawing) while the flow of the gas evacuated through the outlet 22 of the discharge line 15 is measured by the sensor 20.

30 When the valve 14 is opened and the valves 16 and 17 are closed the system functions as an open system without rebreathing.

The system is prepared by blowing into the system a first gas, in this example of an embodiment pure oxygen, by means of the apparatus 11. The apparatus 11 is provided in the part of the line system that is situated behind the third valve 17.

5 The second valve 16 and the third valve 17 are open. Further the first valve 14 is open. Through the discharge 15 and the outlet 22 of the discharge 15 the gas is discharged out of the system. After this by means of the apparatus 11 the system is flushed with 100% oxygen. In the complete line system 95-100% oxygen now is present. After this the second valve 16 and the third valve 17 are closed. The system
10 now functions as an open system. In the part 19 of the line system that is closed off more than 95% oxygen is present. The patient is now connected to the line system and the lungs subsequently are "washed clean" with 100% oxygen.
After this a second gas, an anesthetic gas, such as for instance xenon, or a second mixture of gases, is blown into the line system by the apparatus 11. After the
15 washing clean one wants to obtain the correct concentration of the desired gas in the lungs of the patient in a quick and safe manner. By feeding into the line system 4 a mixture of oxygen and xenon the line system will be filled from the position of the apparatus 11 up to the patient 7 with oxygen and xenon. In the closed off section 9 only oxygen or substantially only oxygen will be present. In the part of the line
20 system situated at the connection to the patient 7 the apparatus 8 is provided, by means of which at the mouth of the patient 7 the concentration of xenon is measured. In this manner it is determined when the line system 4 up to the patient 7 has become filled with a predetermined mixture of xenon/oxygen. When this is the case, the valve 14 is closed and the valves 16 and 17 are opened. The system now goes on to
25 function as a closed system.

Instead of the measuring of the arrival of xenon at the mouth of the patient, and the afterwards closing of the valve 14 and the opening of the valves 16 and 17, one can also choose to feed by means of the apparatus 11 into the line system a
30 predetermined amount of xenon and to subsequently close the valve 14 and to open the valves 16 and 17. In that case the switching of the valves 14, 16 and 17 does not take place in dependence of a measurement at the mouth of the patient.

After the system has gone on to function as a closed system the circulation blower 18 quickly mixes the gases in the closed off section 19 and the other part of the line system 4 with each other, through which the desired mixture is quickly obtained. To that end the circulation blower 18 is provided with a capacity that is such that by means of it a very fast mixing of the gases can take place. The circulation blower 18 has to circulate sufficiently so that the fastness of the mixing process is greater than the fastness of the processes within the human.

In this example of an embodiment the volume of the line system is 2,5 litre while in the line system a circulation blower 18 is provided with in this example of an embodiment a capacity of 60 litre per minute. This leads to a duration of one circulation of the gas of: $2,5 \text{ liter} / 60 \text{ liter/min} = 0.042 \text{ minutes} = 2,5 \text{ seconds}$.

Taking 2,5 seconds as a guiding principle, in the case of for instance a volume of the line system of 1,25 litre a circulation blower having a capacity of 30 litre per minute has to be applied, in the case of a volume of the line system of 5 litre a circulation blower having a capacity of 120 litre per minute has to be applied, and in the case of a volume of the line system of 0,625 litre a circulation blower having a capacity of 15 litre per minute has to be applied.

By the use of the circulation blower 18 a very fast mixing is obtained of the oxygen between the valves 16 and 17, the high percentage of oxygen in the lungs, the section between the patient and the first valve 14 filled with mainly oxygen and the section of the line system 4 between the apparatus 11 and the patient 7. Through this the necessity of prolonged washing is avoided, by which much of the special gas is lost, while a very short washing in time and a safe washing in are realised.

With the method and apparatus according to the invention the fast circulation by the circulation blower is of importance. The control of the composition of the respiratory gas by means thereof can be quicker than the processes in the human. Also because of this the intake of oxygen by the patient can be measured in an accurate manner.

With the closed system according to the invention it is further possible to wash quickly, through which the composition of the respiratory gas can be changed

quickly. The apparatus 11 provides the supply of oxygen in the system and the supply of laughing gas. The pressure in the line system 4 is controlled by the means for the varying of the pressure. The flow through the discharge line 15 and the outlet 22 to outside is, in the half closed system, determined by the flow of fresh gas coming out of the apparatus 11, the movement of the means for the varying of the pressure and the position of the regulating valve 20 in de discharge line 15.

The regulating valve 20 in the discharge line 15 is intended to narrow or in the given case close at the moment the patient breathes in, so that the gas flow 5 does not become negative and the patient therefore only breathes in fresh gas. By means of the sensor 21 the volume or the flow of the gas flowing through the regulating valve 20 is measured.

It is further possible to replace, after the switching to the closed system, the amount of oxygen taken in by the patient by xenon only, and to decrease in this manner the concentration of oxygen and to proportionally increase that of xenon until the desired concentrations are reached. In this manner one saves on the "washing gas" that is discharged.

Instead of xenon any gas mixture can be taken, whereby the concentration of at least two gases can be chosen within narrow boundaries, for instance a xenon/helium mixture. By introducing xenon into the line system while the first valve 14 is open and the valves 16 and 17 are closed, determining the arrival of xenon at the mouth of the patient and subsequently closing the valve 14 and opening the valves 16 and 17 and to switch in this manner from the open to the closed system, there will occur no loss of xenon, while by means of the quick circulation and mixing a homogenous mixture quickly comes into being, and a very short washing in time and a safe washing in are obtained.

30

The embodiments of the present invention for which an exclusive property or privilege is claimed are defined as follows:

1. A respirating apparatus for patients, for anesthesia through inhalation and for administering of therapeutic gases through inhalation, which apparatus is provided with means for circulating a breathing gas, an anesthetic gas or a therapeutic gas in one direction in a line or conduit system, with means for varying a pressure in the line system in accordance with a certain respirating pattern, with means for measuring a flow of the gas and a composition of the gas, whilst the line system is provided with connecting means for a patient and with one or more supplies for various components of a respiratory gas and with means for withdrawing of carbon dioxide exhaled by the patient in the line system, whereby the line system further is provided with a connecting means to a discharge line that is provided with a first closing device for discharge out of the line system of breathing gas, whilst in the line system, as seen in a direction of circulation of the gas, behind the connecting means to the discharge line a second closing means is provided, characterized in that, as seen in the direction of circulation of the breathing gas, behind the second closing means and at a distance therefrom a third closing means is provided, whilst means are provided by means of which the second and third closing means can be controlled in such a way, that a part of the line system situated between the second closing means and the third closing means can be closed off, whilst the line system further is provided with means for generating a gas flow.
2. The apparatus according to claim 1, wherein a capacity of the means for generating the gas flow is adapted to a volume of the line system in such a way, that a duration of one circulation of the gas is 10 seconds at the most.
3. The apparatus according to claim 1, wherein a capacity of the means for the generating the gas flow is adapted to a volume of the line system in such a way, that a duration of one circulation of the gas is 5 seconds at the most.
4. The apparatus according to claim 1, wherein a capacity of the means for generating the gas flow is adapted to a volume of the line system in such a way, that a duration of one circulation of the gas is 3 seconds at the most.
5. The apparatus according to claim 1, wherein the duration of one circulation is 2.5 seconds at the most.

6. The apparatus according to claim 1, 2 or 3, wherein the means for generating the gas flow consists of a circulation blower.
7. The apparatus according to any one of claims 1 to 6, wherein the means for generating the gas flow is provided in a part of the line system that, as seen in the direction of the flow of the breathing gas, is situated behind the second closing means.
8. The apparatus according to claim 7, wherein the means for generating the gas flow is provided in the part of the line system that is situated between the second closing means and the third closing means.
9. The apparatus according to any one of claims 1 to 8, wherein at least one of the first, second or third closing means is formed by a valve.
10. The apparatus according to any one of claims 1 to 9, wherein the supply line or supply lines of the various components of the respiratory gas in the line system are provided in the part of the line system that is situated behind the second closing means.
11. The apparatus according to any one of claims 1 to 10, wherein the means for withdrawing of carbon dioxide exhaled into the line system by the patient is provided in the part of the line system that is situated between the second closing means and the third closing means.
12. The apparatus according to any one of claims 1 to 11, wherein the means for measuring the flow of the gas and the composition of the gas is provided in the part of the line system that is situated at the connecting means for the patient.
13. The apparatus according to any one of claims 1 to 12, wherein the means for measuring the flow of the gas is provided in the part of the line system that, as seen in the direction of the flow of the breathing gas, is situated behind the means for varying the pressure in the line system.
14. The apparatus according to any one of claims 1 to 13, wherein the discharge line is provided with means for measuring of the flow of the gas.

15. The apparatus according to any one of claims 1 to 14, wherein the discharge line for the discharge out of the line system of the respiratory gas is provided with a regulating valve.
16. The apparatus according to any one of claims 1 to 15, wherein the discharge line for the discharge out of the line system of the respiratory gas is provided with a sensor by means of which the flow or the volume of respiratory gas that is flowing through the discharge line can be measured.

