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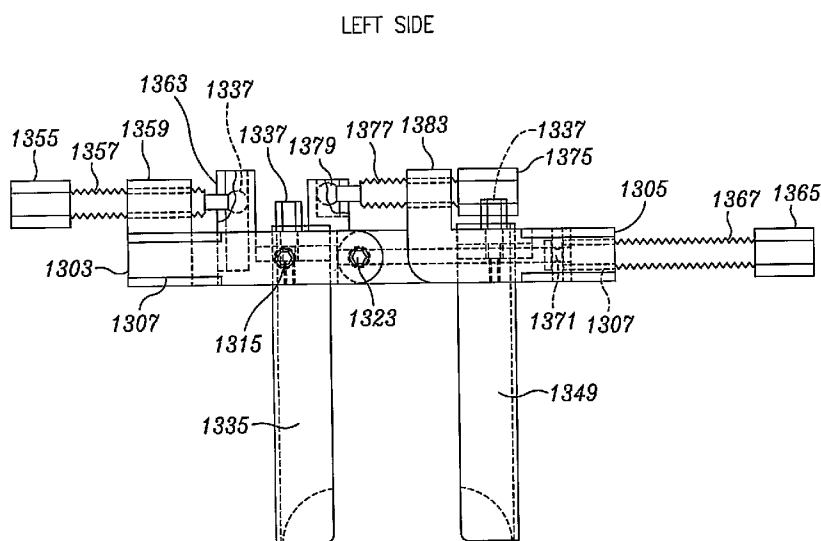
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(54) Title: MINIMAL INCISION MAXIMAL ACCESS MIS SPINE INSTRUMENTATION AND METHOD



(57) Abstract: A minimal incision maximal access system (573, 631, 657, 691, 751, 901, 1001, 1301, 1801) allows for maximum desirable work space exposure within the incision along with maximum access to the operative field utilizing a minimum incision as small as the width of the working tube. Instead of multiple insertions of dilating tubes the design is a streamlined single entry device to avoid repetitive skin surface entry. The system offers the capability to expand to optimum exposure size for the surgery utilizing retractors depending from a bi-hinged frame having internal or external controls to control the angle and separation of the retractors. Interchangeable retractor blades can be attached to the frame. At least one retractor blade is independently controlled.

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**MINIMAL INCISION MAXIMAL ACCESS
MIS SPINE INSTRUMENTATION AND METHOD**

Field of the Invention

The present invention relates to improvements in the field of minimal invasive surgery and more particularly to instrumentation which allows for maximal access to the surgical field through the smallest possible incision. Greater access is allowed into the working field while enjoying the reduction of trauma and disturbance to surrounding tissues, which results in a reduced time necessary to complete the operative procedure, increased safety of the procedure, and further patient recovery and rehabilitation, as well as less blood loss. Further, increased accuracy by providing an expanded working field is another goal to help the surgical practitioner perform well within a short time.

Background of the Invention

Microscopic Lumbar Discectomy techniques were developed and championed by Dr. Robert Williams in the late 1970's and by Dr. John McCullough in the late 1980's and 1990's. For the first time since the advent of Lumbar Disc Surgery by Mixter and Barr in 1934 a method was introduced allowing Lumbar Disc Surgery to be performed through a small incision safely resulting in faster patient recovery and converting a two to five hospital stay procedure virtually to an outpatient procedure.

The special retractors developed by Drs. Williams and McCullough however were often difficult to maintain in optimum position and relied on the interspinous and supraspinatus ligaments for a counter fixation point severely stretching the structures. This stretching along with the effects of partial facetectomy, discectomy, removal of the ligamentum flavum and posterior longitudinal ligament contributed to the development of Post Discectomy Instability. Taylor retractors were also used but were cumbersome, required larger incisions and often

injured the facet joints.

Dr. William Foley in 1997 introduced a tubular system mated to an endoscope which he labeled a Minimal Endoscopic Discectomy (MED) system. It featured sequentially dilating the Lumbar Paraspinous Muscles allowing a working channel to be advanced down to the level of operation through which nerve root decompression and Discectomy Surgery could be performed with a small incision and less muscle trauma. Improvements were made by Dr. Foley in his second generation METRx system. However, there were several disadvantages to the MED and METRx systems.

In the MED and METRx systems, the cylindrical working channel considerably restricted visualization and passage of instruments. It also compromised the "angle of approach" necessary for safe usage of the operating instruments. This problem was proportionately aggravated with the long length of the tube. This compromised visualization contributed to the following problems, including nerve injury, dural tear, missed disc fragments, inadequate decompression of the lateral recess, increased epidural bleeding, difficulty controlling epidural bleeding, inadequate visualization of the neuroforamen, and inadequate decompression of neuroforamen.

The repetitive introduction of successively larger dilators caused skin abrasion with the potential for carrying superficial skin organisms down to the deeper tissue layers hypothetically increasing the risk of infection. The learning curve for operating in a two dimension endoscopic field proved to be arduous and contributed to the above complications.

The attempted use of the METRx system for more complex procedures such as fusion was further hazardous by inherent limitations. Endius in September of 2000 then introduced a similar device which differed by having an expandable foot piece to allow greater coverage of the operative field. However, the enlarged foot piece was unwieldy and difficult to seat properly. Exposure of the angle of approach was also limited by having to operate through a proximal cylindrical tube with its limitations as described before. In comparison

to the METRx system the working area was improved but access was again restricted by the smaller proximal cylinder.

Both systems offered endoscopic capability but many spine surgeons chose to use an operating microscope or loupes to maintain 3-Dimensional visualization rather than the depth impaired 2-Dimensional endoscopic presentation. Keeping debris off of the endoscopic lens has also proved to be a troubling challenge.

More recently several MIS Retractors have been designed for general and spine surgery (Nuvasive, Danek-Quadrant, Depuy-Pipeline). There have also been modifications of older devices offering to enter the arena of MIS Spine Surgery (Koros). The plethora of proposed surgical retraction devices and methods have led to a confusion of meaning of the "MIS Surgical Technique." Surgical incisions of up to five inches in length have been described for MIS Surgery. Usage of the term "MIS Surgery" as applied to spine surgery, appears to have evolved to mean a surgical incision less than the traditional one or two levels above and below the surgical field of interest. However, the combined length of two incisions (right and left) often is longer than the single midline incision. The true advantage of MIS Surgery over the traditional technique is the specificity of exposure such that only the required amount of retraction of soft tissue is used to safely accomplish the specific surgical procedure.

Ideally, there are certain prerequisites for a MIS spine retractor that should be fulfilled in order to accomplish the objective that only the required amount of retraction of soft tissue is used:

1. The retractor must provide sufficient direct visualization of the neural elements, related blood vessels, and bony landmarks to accomplish safe spine surgery.
2. The retractor should require the least amount of resection of adjacent tissue muscle, fascia, bone, and joints to accomplish the task.
3. The retractor should be self-retaining instead of

- hand-held (Ritland).
4. Deployment of the surgical retractor should be able to be prompt and precise in location.
 5. The retractor should be easy to adjust for length, width, and angle of exposure.
 6. The retractor support, such as a frame, must have the capability to lie flat to the surface contour of the body so that the attached retractor blades could be as short as possible.
 7. The retractor support, such as a frame and blades must be stable once optimum surgical exposure is obtained.
 8. There should be a minimum of "fiddle factor" so the surgeons attention can remain focused on the 0-ion and not distracted by the complexity of using the retractor.
 9. The retractor must be "strong enough" in design not to flex and lose exposure.
 10. Particularly for surgery of the posterior lumbar spine, the retractor must be designed to counter the powerful paraspinal muscle resistance without using large incremental changes (e.g. widely spaced ratcheted gap).
 11. With longer exposure length, there must be an efficient means to retract muscle that encroach between the retractor blades.
 12. The need for ancillary equipment such as light source attachments, etc., are self evident

Currently available surgical retractor systems fail to fulfill of the above requirements. Consequently there is a severe need for structures and procedures to meet such requirement.

Due to the spine surgeon's desire to utilize the advantages of MIS Surgery to evermore complex procedures, the MIS Surgical Retractors have evolved to attempt accommodate this need. For example. the Danek MED Tube evolve to the X-Tube and then to the Quadrant system (U.S. Patent No. 6,945,933 to

Branch et. al). Still other retractor inventions have come to market including the three-bladed, Nuvasive design for the lateral approach to the Lumbar Interbody Space, the Depuy "pipeline" retractor, a highly complex four-bladed retractor system with a curved ratchet arm, the Stryker Luxor. None of the above retractor Systems incorporate the full complement of prerequisites listed above.

The Quadrant System with its sequential dilating tube method of introduction into the body encounters problems when the retractor blades are opened apart. As the strong fascia and paraspinal muscle have remained intact, a monumental battle develops between the separating blades and the intact muscle and fascia resisting the expansion. This necessarily results in tearing and shredding of the muscle as the blades are forced apart. The Quadrant System is also based on a straight bar with a ratchet devise and therefore cannot accommodate the Lumbar lordosis which can approximate forty degrees at the lumbosacral junction. This requires retractor blades to be longer as the frame tends to "ride up from the surface of the skin".

The retraction blades of the Quadrant system are also a considerable distance from the ratchet bar creating unwanted movement, stress, and loss of muscle retraction compromising exposure. The Quadrant system's retractor blades location at a considerable distance from its base attachment point on its ratchet bar creates a long lever arm moment which lends to such instability of the retractor blades. The Branch reference also shows a curved frame but this cannot adjust to different lordotic angles of the patient.

Pipeline retractor has the deficiencies as described in the Quadrant System, and suffers from negative effects of its extreme complexity. First, the pipeline retractor (Raymond et al) also shows curved ratchet arms to accommodate the lumbar lordosis. Again their fixed curvature cannot adjust to different lordotic angles. Secondly, the Pipeline retractor has proven to extremely difficult to spread the retractor

blades up an inclined slope along the arc of the ratchet arms against the strong resistance of the muscle and fascia even using a separate spreader device. Thirdly, the pipeline device is so complex that it is very difficult and time consuming to set up and operate.

The Nuvasive retractors also has the deficiencies as described for the Quadrant System but, Nuvasive also suffers from an inherent disadvantage of a three bladed retractor system. If the Nuvasive retractor is deployed such that the middle blade is lateral, then visualization of the spinal canal can be difficult. If the Nuvasive middle blade is placed medial, there is significant muscle encroachment as the blades are spread apart.

in the case of the (split) Pipeline System and an inherent disadvantage of a three bladed retractor system in the case of Nuvasive. If the Nuvasive retractor is deployed such that the middle blade is lateral, then visualization of the spinal canal can be difficult. If the Nuvasive middle blade is placed medial, there is significant muscle encroachment as the blades are spread apart.

Another reference, U.S. Patent No. 6,224,545 to Cocchia has a number of shortcomings, including (1) a surgical frame having no structure to allow flexion and extension, (2) retractor blades which are rotated with an awkward force plate device, and (3) the knobs are used to control movement of the device are difficult to use due to the proximity on the patient's skin and inability to apply adequate torque.

Summary of the Invention

The system and method of the invention, hereinafter minimal incision maximal access system, includes a surgical operating system that allows for maximum desirable exposure along with maximum access to the operative field utilizing a minimum incision as small as the METRx and Endius systems. The minimal incision maximal access system disclosed offers

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advantages over the METRx and Endius systems in several respects. First, instead of multiple insertions of Dilating Tubes the Invention is a streamlined single entry device. This avoids repetitive skin surface entry. Second, the minimal incision maximal access system offers the capability to expand to optimum exposure size for the surgery utilizing hinged bi-hemispherical or oval Working Tubes applied over an introducer Obturator which is controllably dilated to slowly separate muscle tissue.

Third, the minimal incision maximal access system maximizes deeper end working and visualization area with maximum proximal access and work dimensions significantly greater than either the METRx or Endius devices and methods. Fourth, the minimal incision maximal access system provides expanded visual and working field to makes the operative procedure safer in application and shorten the surgeons's learning curve because it most closely approximates the open microdisectomy techniques. Fifthly, the minimal incision maximal access system has a tapered ended Obturator which allows for tissue spread rather than muscle tissue tear and subsequent necrosis.

Sixth, the minimal incision maximal access system controls muscle oozing into the operative field which is controlled by simply opening the tubes further. This also thereby controls the bleeding by pressure to the surrounding tissues. Seventh, in contrast to the cylindrical tube based systems such as the METRx and Endius the minimal incision maximal access system offers a larger working area in proportion to the working depth. For the first time this allows for a minimal access technique to be applied to the large or obese patients. The enlarged footprint of the longer tubes in the minimal incision maximal access system is a major difference from any other minimal access system.

An eighth advantage of the minimal incision maximal access system is that the expandable design allows for excellent exposure for more complex procedures such as fusion and instrumentation including TLIF, PLIF, and TFIF (Transfacet

Interbody Fusion), as well as allowing application for surgery on other areas of the body. For example, minimal incision maximal access system can be used for cervical surgery posteriorly (foraminotomy, lateral mass instrumented fusion) as well as anteriorly for a cervical discectomy and fusion. The minimal incision maximal access system can also be used for anterior lumbar interbody fusion be it retroperitoneal, transperitoneal or laparoscopic from anterior or lateral approaches.

A ninth advantage of the minimal incision maximal access system is that the medial oval cutout of the retractor blade forming the working tube, allows more central docking on the spine which is problematic for other devices. A medialized docking provides access for easier and better and safer dural retraction to address midline pathology. A tenth advantage is had by including an anti-reflective inner surface of the retractor blades which eliminates unwanted glare.

An eleventh advantage of the minimal incision maximal access system includes the slanted and contoured distal end of the retractor blade which allows minimal resistance for entry and advancement to the docking site. A twelfth advantage minimal incision maximal access system is the provision of a variety of retractor tips specific for different surgical procedures.

A thirteenth advantage of the minimal incision maximal access system is the provision of oval or more flatter shaped retractor blades for larger access requirements such as pedicle to pedicle exposure and especially in the case where pedicle screw instrumentation is to be applied. This minimizes unnecessary muscle spread by providing a smaller waist profile than a circular system. A fourteenth advantage of the minimal incision maximal access system is that the larger retractor blade also features one or two "skirts" to cover the lateral aperture created by the spread of the two retractor blades when opened. This prevents soft tissue and muscle ingress into the exposure zone. The skirts are attached to the working tube either at the hinge or on one or both of the two halves of the

retractor blades.

A fifteenth advantage of the minimal incision maximal access system is the provision of a modular design in which the retractor blades can be quickly removed, changed and reapplied. In this version the proximal port can also be modular and changeable to fit the needs of a specific surgical procedure.

A sixteenth advantage of the minimal incision maximal access system is that the retractor blades can be made out of metal, ceramic or plastic, can be opaque or translucent, and can have tips of different shapes for different applications.

A seventeenth advantage is the provision of snap lock connections of the major parts of the Invention provides for easy assembly and disengagement for cleaning and sterilization purposes.

An eighteenth advantage is that the Obturator is cannulated for carrying a central Guide Pin Passage. It has a Handle component which remains superficial to the skin. The obturator houses an internal hinge device which allows for spread of the two obturator tips.

A nineteenth advantage is the uniquely designed facial incision and dissection which creates the least traumatic way to traverse the muscle layer by incision of the firm fascia and aponeurosis splitting the muscle in the direction of its fibers and the technique of detaching the muscle attachment to the bone rather than tearing and ripping of the muscle.

A twentieth advantage involves the possibility that the improved retractor can range in complexity from a single axis dual hinged, two-blade retractor which allows not only expansion at the deep end of the retractor blades, but also expansion at the top end.

A twenty first advantage is the use of a simple modification of a Gelpi-type retractor enables retraction in the other direction.

A twenty second advantage is that in further embodiments, a double support, such as a frame can be connected by a controllable hinge which allows flexion and extension to accommodate the contour of the patient's body surface.

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A twenty third advantage is that the retractor blades are interchangeable and have independent control features.

A twenty fourth advantage is that overall, the focus of this invention's design has been to maintain simplicity and efficiency in the use of the retractor.

A twenty fifth advantage of our approach (both retractor and surgical) is achieved by incising the fascia and spreading the muscle in the direction of its fibers before the retractor is deployed.

In contrast to the shortcomings of presently commercially available retractors, the inventive retractor offers the following advantages:

1. Atraumatic one step entry into the body.
2. Pre-deployment soft tissue is released in a controlled least-traumatic fashion.
3. Streamlined retractor design can accomplish tissue retraction with only three controls.
4. Microcontrol feature with a simple screw-activated design gives precise control and mechanical advantage.
5. In one embodiment, a "hands away horn the body design" utilizes an innovative ratchet.
6. The frame/support is connected by micro-adjustable hinge to customize flexion or extension to match the body contour.
7. Customized retractor blade tips to "dock" to the surgical work site.
8. Modular, easy to change design for the retractor blades and tips.
9. Method to retract muscle ingress by customized deep Gelpi-type retractor customized for use with the retractor of the invention.
10. MIS retractor design applicable for surgery to several areas of the body and specifically for the lumbar spine allowing access for up to a three level instrumented fusion which is not currently possible with any other MIS spinal retractor.

Brief Description of the Drawings

The invention, its configuration, construction, and operation will be best further described in the following detailed description, taken in conjunction with the accompanying drawings in which:

Figure 1 is a perspective view of a working tube with an angled upper section and shown in position with respect to an obturator insertable into and workable within the working tube;

Figure 2 is a perspective assembled view illustrating the relative positions of the obturator and working tube;

Figure 3 is a perspective assembled view illustrates the position of the obturator after it has been inserted into the working tube;

Figure 4 is a view taken along line 4 - 4 of Figure 2 and looking into the working tube of Figure 1;

Figure 5 is a sectional view taken along line 5 - 5 of Figure 2 and looking into the hinge of working tube of Figure 1, illustrating its hinge connections;

Figure 6 is an side end view of the working tube of Figures 1-5 and illustrating predominantly one of the rigidly connected halves of the invention;

Figure 7 is a side sectional view taken along line 7 - 7 of Figure 6 and showing the internal bearing pivot;

Figure 8 is a side sectional view taken along line 8 - 8 of Figure 5 and illustrating a option for external bevel for the working tube;

Figure 9 is a side view of the working tube of Figures 1-8 shown with the lower portions in parallel alignment and the upper portions angled with respect to each other;

Figure 10 is a side view of the working tube as seem in Figure 9 and shown with the lower portions in an angled relationship and the upper portions in a closer angled relationship with respect to each other;

Figure 11 is a side view of the working tube as seen in Figures 9 and 10 and shown with the lower portions in a maximally angled relationship and the upper portions in parallel alignment signaling maximal spread of the lower

portions in bringing the upper portions into parallel alignment;

Figure 12 is a side view of the obturator of Figure 1 and seen in an assembled view and emphasizing a through bore seen in dashed line format;

Figure 13 is a side view of the obturator of Figure 11 as seen in an assembled view but turned ninety degrees about its axis and emphasizing the through bore;

Figure 14 shows a side view of the obturator 33 of Figure 13 with the spreading legs in an angled apart relationship;

Figure 15 is a sectional view taken along line 14 - 14 of Figure 12 and gives a sectional view from the same perspective seen in Figure 14;

Figure 16 is a view of the obturator similar to that seen in Figure 15, but turned ninety degrees along its axis and illustrates the wedge as having a narrower dimension to lend internal stability;

Figure 17 is a closeup view of the external hinge assembly seen in Figure 1 and illustrates the optional use of a plug to cover the exposed side of a circular protrusion;

Figure 18 is a view taken along line 18 - 18 of Figure 11 and illustrates the use of an optional skirt having flexible members which spread from an initial curled position to a straightened position to better isolate the surgical field;

Figure 19 is a view of the lower tube hemicylindrical or curved portions 65 and 69 in a close relationship illustrating the manner in which the skirts sections within their accommodation slots areas;

Figure 20 is a cross sectional view of the a patient and spine and facilitates illustration of the general sequence of steps taken for many procedures utilizing the minimal incision maximal access system disclosed;

Figure 21 illustrates a fascial incisor over fitting a guide pin and further inserted to cut through external and internal tissue;

Figure 22 illustrates the assembled Working Tube - Obturator being inserted into the area previously occupied by

the fascial incisor and advanced to the operative level lamina;

Figure 23 illustrates the obturator 33 being actuated to a spread orientation to which automatically actuates the working tube to a spread orientation;

Figure 24 is a view of the working tube 35 is in place and supported, held or stabilized in the field of view by a telescoping support arm and engagement, the opposite end of the stabilizing structure attached to the operating table;

Figure 25 illustrates further details of the support arm seen in Figure 24, especially the use of a ball joint;

Figure 26 illustrates a side view of the assembly seen in Figure 25 is seen with an adjustable clamp operable to hold the working tube open at any position;

Figure 27 is a top view looking down upon the adjustable clamp seen in Figures 25-26 and shows the orientation of the working tube and adjustable clamp in fully closed position;

Figure 28 shows a variation on the obturator seen previously in Figure 1 and illustrates the use of handles which are brought together;

Figure 29 illustrates a further variation on the obturator seen previously in Figure 1 and illustrates the use of a central ball nut;

Figure 30 is a sectional view taken along line 30 - 30 of Figure 29 and illustrates the use of a central support block to support the central threaded surface;

Figure 31 is a top view of a thin, inset hinge utilizable with any of the obturators herein, but particularly obturators of Figures 1 and 29;

Figure 32 is a sectional view of the obturator of Figure 1 within the working tube of Figure 1 with the wedge 51 seen at the bottom of an internal wedge conforming space;

Figure 33 illustrates the obturator seen in Figure 32 as returned to its collapsed state.

Figure 34 illustrates a top and schematic view of the use of a remote power control to provide instant control of the working tube using an adjustable restriction on the upper angled curved portions of the working tube;

Figure 35 is a view taken along line 35 - 35 of Figure 34 and illustrating the method of attachment of the cable or band constriction;

Figure 36 is a mechanically operated version of the nut and bolt constriction band seen in Figure 25;

Figure 37 is an isolated view of two curved tube sections shown joined in a tubular relationship and indicating at least a pair of pivot axes on each curved tube section;

Figure 38 is an isolated view of two curved tube sections as seen in Figure 38 which are angularly displaced apart about a shared first pivot axis on each of the curved tube sections;

Figure 39 is an isolated view of two curved tube sections as seen in Figures 38 and 39 which are angularly displaced apart about a shared second pivot axis on each of the curved tube sections;

Figure 40 is a plan view of a given width supplemental side shield having a width of approximately the separation of the curved tube sections as seen in Figure 39;

Figure 41 is a top view of the supplemental side shield of Figure 40;

Figure 42 is a pivoting thread support system in which a pair of opposing flank threaded members operate a pivoting support and are connected by a gear mechanism shown in exaggerated format to give single knob separation control;

Figure 43 illustrates a surrounding support system utilized to provide and enable pivoting and translation;

Figure 44 illustrates a view looking down into the structure of Figure 43 shows the overall orientation and further illustrates an optional securing tang;

Figure 45 illustrates a simplified control scheme in which simplicity is emphasized over controllability with less moving parts and expense;

Figure 46 illustrates a further embodiment of a manipulative structure which works well with the structure of Figure 45;

Figure 47 illustrates another possible realization which combines the control mechanisms of selected portions of Figures

37 - 46, combined with other possible options;

Figure 48 illustrates a side view of the side shield seen in Figure 47;

Figure 49 illustrates one possible configuration for a variable depth guide which is utilizable with any of the devices seen in Figures 37 - 46 or any other tubular, minimally invasive system;

Figure 50 is a vertical plan view of an expandable frame system which uses detents to set the frame size and which uses an angular distribution system;

Figure 51 is a top view of the system of Figure 51 in an expanded position;

Figure 52 is a side view of the system of Figures 50-52;

Figure 53 illustrates a top view double pivot hinge fitting and illustrating the gear surfaces;

Figure 54 illustrates the action of the pivot hinge which produces an even angular deflection;

Figure 55 illustrates a top view of a bookwalter device mounted atop a central hinge box seen in Figure 53;

Figure 56 is a top view of a retractor system employing many of the components seen in Figures 50-52 for applying force from a distance;

Figure 57 is a top view of a curved retractor tube extension;

Figure 58 is a side sectional view of the curved retractor tube extension of Figure 57 attached to the curved tube seen in Figure 52;

Figure 59 is a view looking down into the inside of the curved retractor tube extension of Figures 57 and 58;

Figure 60 is a view looking down onto the outside of the curved retractor tube extension of Figures 57-59;

Figure 61 is an exploded view of a further embodiment of a frame retractor system utilizing a base frame and raised tube manipulator;

Figure 62 is a perspective view of the frame retractor system seen in Figure 61;

Figure 63 is a perspective view of the frame retractor

system from the same perspective as seen in Figure 61 and illustrated as being fitted with a fiber optic illuminator;

Figure 64 is a top view of the frame retractor system seen in Figures 61-63;

Figure 65 is a bottom view of the frame retractor system seen in Figures 61-64;

Figure 66 is a side view of the frame retractor system seen in Figures 61-65;

Figure 67 is a perspective view of a wire retractor utilizable with the frame retractor system of Figures 61-67;

Figure 68 is an isolated view of the ends of the wire retractor shown in an opening pattern;

Figure 69 is an isolated view of the ends of the wire retractor shown superimposed in a crossing pattern to reduce the profile for entry into the frame retractor system of Figures 61-66;

Figure 70 is a side view of the frame retractor system seen in Figures 61-63, and illustrating portions of an optional wire guide retractor;

Figure 71 illustrates the frame retractor system and wire retractor shown with respect to tissue;

Figure 72 illustrates the wire retractor being opened to an open position within the frame retractor system and within the tissue;

Figure 73 illustrates a plan view of a manual tool with a main handle portion and interfitting blades;

Figure 74 illustrates a different interchangeable blade attachment for the manual tool of Figure 73;

Figure 75 is a further embodiment of the manual tool seen in Figures 73 and 74;

Figure 76 illustrates a view looking into the slip fitting of the manual tool of Figure 75;

Figure 77 illustrates a top view of a further embodiment of a frame retractor system;

Figure 78 illustrates a bottom view of the embodiment of Figure 77;

Figure 79 illustrates a sectional view taken along line

79-79 of Figure 77;

Figure 80 illustrates a sectional view taken along line 80-80 of Figure 77;

Figure 81 a top semi sectional detail view of the inside corner of the first inner translatable frame member seen in Figures 77 & 78 and shown in locked position;

Figure 82 is a view in accord with Figure 81 but illustrating the unlocked position;

Figure 83 illustrates a top view of a first generally curved retractor member utilizable with a frame retractor system;

Figure 84 illustrates a top view of a second retractor member which may be utilizable with the first retractor member of Figure 83;

Figure 85 illustrates a left side view of the first retractor member of seen in Figure 83;

Figure 85 illustrates a right side view of the second retractor member of seen in Figure 84;

Figure 87 illustrates a rear view of the second retractor member of Figures 84 and 86;

Figure 88 illustrates a top view of a first generally rectangular profile retractor member having curved edges and utilizable with a frame retractor system;

Figure 89 illustrates a top view of a second retractor member utilizable with the first retractor member of Figure 88;

Figure 90 illustrates a left side view of the first retractor member of seen in Figure 88;

Figure 91 illustrates a right side view of the second retractor member of seen in Figure 89;

Figure 92 illustrates a rear view of the second retractor member of Figures 89 and 91;

Figure 93 illustrates a right side view of the a retractor member having a bulge near its lower extent;

Figure 94 illustrates a rear view of the retractor member of Figure 93;

Figure 95 illustrates a right side view of the a retractor member having a grossly but gently serrated lower shape;

Figure 96 illustrates a rear view of the retractor member of Figure 93;

Figure 97 illustrates a right side view of the a retractor member having a rounded cutout at its lower edge;

Figure 98 illustrates a rear view of the retractor member of Figure 97;

Figure 99 is a left side view of the frame retractor system of Figures 77 to 82 in which the retractor members are shown parallel and separated from each other;

Figure 100 is a right side view of the frame retractor system similar to that seen in Figure 99 and in which the retractor lower extension members are shown parallel and separated from each other;

Figure 101 is a right side view of the frame retractor system similar to that seen in Figures 99 to 100 and showing angular displacement of the first main frame member with respect to the second main frame member;

Figure 102 is a right side view of the frame retractor system similar to that seen in Figures 99 to 101 and showing angular displacement of the first inner pivotable frame member causing the lower extension members to angle away from each other;

Figure 103 is a right side view of the frame retractor system similar to that seen in Figures 99 to 102 and showing angular displacement of the first inner pivotable frame member causing the lower extension members to angle toward each other;

Figure 104 is a right side view of the frame retractor system similar to that seen in Figures 99 to 103 and showing retractor lower extension members parallel and adjacent each other;

Figure 105 is a right side view of the frame retractor system similar to that seen in Figures 99 to 104 and showing retractor lower extension members parallel and displaced from each other;

Figure 106 illustrates a top view of frame retractor system similar to that seen in Figures 99 to 105 and showing retractor lower extension members parallel and in adjacent

relationship as seen in Figure 104;

Figure 107 illustrates a right side view of frame retractor system similar to that seen in Figures 99 to 106 and showing an obturator used in conjunction with the frame retractor;

Figure 108 illustrates a left side of the frame retractor system similar to that seen in Figures 99 to 107 and showing disengagement of the angular displacement mechanism to permit free angular movement;

Figure 109 illustrates a top view of a variation on the frame retractor system in Figures 99 to 108 as having two external controls moved inside the outer surface of the frames and including a worm gear system for angular adjustment of the retractor members and first and second main frame members;

Figure 110 is a bottom view of the retractor system seen in Figure 109;

Figure 111 is a bottom view of the retractor system seen in Figures 109 and 110;

Figure 112 is a left side view of the retractor system seen in any of the Figures 99 to 111 and in which the obturator and working blade of Figure 1 is supported by the first and second main frame members where the interfitting retractor members have been removed;

Figure 113 is a top view of the arrangement seen in Figure 112;

Figure 114 illustrates a side view looking into and partially through a ratchet actuation tool utilizable for force adjustment in a sterile surgical environment;

Figure 115 illustrates a view of the ratchet actuation tool including the first plate & supported components seen with the second plate removed;

Figure 116 illustrates a plan view of the ratchet actuation tool first plate;

Figure 117 illustrates a plan view of the ratchet actuation tool second plate;

Figure 118 illustrates a sectional view taken along the midline of the ratchet actuation tool first plate;

Figure 119 illustrates a sectional view taken along the midline of the ratchet actuation tool second plate;

Figure 120 illustrates an end view looking into the first socket;

Figure 121 illustrates a plan view of the first socket;

Figure 122 is a top end view of the first socket seen in Figures 120 and 121;

Figure 123 is a rear end view of the second socket;

Figure 124 illustrates a plan view of the second socket;

Figure 125 illustrates an end view looking into the second socket seen in Figures 123 and 124;

Figure 126 illustrates a plan view of the ratchet sprocket engagement head;

Figure 127 illustrates an end view of the ratchet sprocket engagement head;

Figure 128 illustrates a plan view of the sprocket;

Figure 129 illustrates a plan view looking downward on the spacer clip; and

Figure 130 is an exploded sectional detail illustrating the relationship of the first and second plates, how the spacer clip is secured to the first plate, how the spacer clip secures the second plate and how the spacer clip acts to control the spacing between the first and second plates.

Detailed Description of the Preferred Embodiment

The description and operation of the minimal incision maximal access system will be best described with reference to Figure 1 and identifying a general system 31, although Figures 1, 2 & 3 should be referenced simultaneously. System 31 includes an obturator 33 and a working tube 35. The orientation of the obturator 33 is in a slightly displaced from a position of alignment with the working tube 35 for entry into working tube 35 and to provide the initial carefully controlled force for spreading the working tube 35, as will be shown.

Obturator includes an upper control housing 37 and a pair of spreading legs 39 and 41. The spreading legs 39 and 41 are seen as coming together to form a conical tip and thus have

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hemi-conical end portions. The spreading legs 39 and 41 over fit the attachment leg portions 43 and 45, respectively. At the top of the upper control housing 37 a boss 47 surrounds and supports the extension of a control shaft 49. A knurled thumb knob 50 sits atop the control shaft 49 to facilitate controlled turning of the control shaft 49 to control the degree of spreading of the spreading legs 39 and 41. Thus spreading can be controlled independently of pressure applied along the length of the obturator 33.

Below the upper control housing 37 is the bottom of the control shaft 49 which operates against a wedge 51. The wedge 51 operates within a pair of opposing slots 52 in an upper portion 53 of the overfit attachment leg portions 43 and 45. The lower ends of the overfit attachment leg portions 43 and 45 include insertion tangs 55 which fit within insertion slots 57 of the spreading legs 39 and 41. The overfit attachment leg portions 43 and 45 are pivotally attached to the upper control housing 37 internally by pivot blocks 59 which fit within access apertures 60.

The working tube 35 has a first lower extending connection tang 61 and a second lower extending connection tang 63. First lower extending connection tang 61 connects into a slot 64 of a lower tube curved portion 65. The first lower extending connection tang 61 is fixed to an upper angled curved portion 67. The second lower extending connection tang 63 connects into a slot 68 of a lower tube curved portion 69. Second lower extending connection tang 61 is fixed to and an upper angled curved portion 71. The upper angled curved portion 67 may have a reinforced wear plate 73 for applying upper pressure and force on the upper angled curved portions 67 and 71 toward each other to cause the first and second lower extending connection tangs 61 & 63 and their connected lower tube curved portions 65 and 69 to be urged away from each other.

At the side of the working tube 35 at the transition between the upper angled curved portions 67 and 71 and at a point just above the first and second lower extending

connection tangs 61 & 63 is an external hinge assembly 77. Hinge assembly 77 may include an optional first guide plate 79 (seen in Figure 2) and first circular protrusion 81 attached to upper angled curved portions 67, and a first slotted plate 83 positioned adjacent to first guide plate 79 and having a slot partially surrounding the circular protrusion 81.

Upper angled curved portion 71 has a pair of spaced apart facing surfaces facing a matching pair of facing surfaces of the upper angled curved portion 67, of which a dividing line 85 is seen. Upper angled curved portions 67 and 71 are brought together to cause the first and second lower extending connection tangs 61 & 63 and their connected lower tube curved portions 65 and 69 to spread apart.

In the view of Figure 1, the first and second lower extending connection tangs 61 & 63 are shown in a spread apart relationship. A locking pin 87 is seen which can be used to engage angularly spaced apart apertures in the circular protrusion 81 to provide a detent action to hold the working tube 35 in various degrees of spread. Also seen is a slight exterior bevel 89 on the lower tube curved portions 65 and 69.

Note the angled separation of the upper angled curved portions 67 and 71. The angle of the opposing surfaces (only opposing surface 91 is seen in Figures 2 & 3) equals the angle of spread of the first and second lower extending connection tangs 61 & 63.

Referring more closely to Figure 2, a perspective assembled view illustrates the relative positions of the obturator 33 and working tube 35 in a position for the obturator 33 to be inserted into the working tube 35 and before any spreading takes place.

Referring to Figure 3, a perspective assembled view illustrates the position of the obturator 33 after it has been inserted into the working tube 35 and again before any spreading takes place. Note that the pivot axes of the first and second lower extending connection tangs 61 & 63 are on par with the pivot axes of the insertion tangs 55. The tip of the obturator 33 extends slightly beyond the bottom most part of

the working tube 35 so that the completed assembly can be smoothly urged past muscle and other tissue.

Referring to Figure 4, a view taken along line 4-4 of Figure 1 is a view looking down into the working tube 35. Other features seen include a wear plate 93 located on the upper angled curved portion 71. In both of the wear plates 73 and 93 a universal port 94 is provided as a bore for insertion of a tool or lever to assist in bringing the upper angled curved portions 67 and 71 into a tubular relationship. Further, an identical hinge assembly 77 on the side opposite that seen in Figure 1 is shown with the same numbering as the components which were seen in Figure 1.

Also seen are the pair of opposing surfaces 91 on upper angled curved portion 71 and a pair of opposing surfaces 97 on upper angled curved portion 67. Also seen is a central working aperture 99.

Referring to Figure 5, a view taken along line 5-5 of Figure 1 is a sectional view looking down into the working tube 35. The connectivity of the structures seen in Figure 4 are emphasized including the connection of circular protrusion 81 to the upper angled curved portion 71, and the connection of first slotted plate 83 to upper angled curved portion 67, and which is indicated by the matching section lines. Further, an identical hinge assembly 77 on the side opposite that seen in Figure 1 is shown with the same numbering as the components which were seen in Figure 1.

Referring to Figure 6, a view of one end of the working tube 35 illustrates predominantly the second angled half portion 63. Elements seen in Figures 1 - 3 are made more clear in Figures 6 - 11.

Referring to Figure 7, a side sectional view taken along line 7 - 7 of Figure 6 and shows the internal bearing pivot consisting of a slightly greater than hemispherical side bump projection 101 located on upper angled curved portion 71, and a slightly less than hemispherical side circular groove 103 located on upper angled curved portion 67. Also seen is the interconnect slots 64 and 68 as well as the first and second

lower extending connection tangs 61 and 63. In the showing of Figure 7 an external bevel 105 is utilized

Referring to Figure 8, a side semi-sectional view taken along line 8 - 8 of Figure 5 illustrates the integral connectivity of circular protrusion 81 with the upper angled curved portion 71. Seen for the first time in isolation are a pair of pin apertures 107 for engaging the locking pin 87.

Referring to Figure 9, an illustration of a side plan view and in which the lower tube curved portions 65 and 69 are in matching straight alignment and forming a lower tube shape, while the upper angled curved portions 67 and 71 are angled apart.

Referring to Figure 10, a midpoint of movement is illustrated wherein the lower tube curved portions 65 and 69 have begun to move apart widening the lower tube shape previously formed into an angled apart opposing curved shape, while the upper angled curved portions 67 and 71 are brought closer together to have a closer though angled apart an angled apart opposing curved shape.

Referring to Figure 11, a completed movement, with respect to the view of Figure 4 illustrates a state where the lower tube curved portions 65 and 69 have moved apart to their maximum extent into a maximally angled apart opposing curved shape, while the upper angled curved portions 67 and 71 are brought completely together to form an upper tube shape. It is the position of Figure 6 which is the ideal working position once the lower tube curved portions 65 and 69 are within the body, and provides an expanded working field at the base of the working tube 35. Surgical work is ideally performed through the upper, abbreviated axial length tube shape formed by the upper angled curved portions 67 and 71.

Referring to Figure 12, a side view of the obturator 33 of Figure 1 is seen in an assembled view and emphasizing in dashed line format a through bore 111 which extends through the obturator 33 from the knurled knob 50 through to the tip of the pair of spreading legs 39 and 41 (leg 41 is not seen in Figure 12).

Referring to Figure 13, a side view of the obturator 33 of Figure 11 is seen in an assembled view but turned ninety degrees about its axis, and again emphasizing in dashed line format the through bore 111 which extends through the obturator 33 from the knurled knob 50 through to the tip of the pair of spreading legs 39 and 41. It is from this position that further actuation will be illustrated.

Referring to Figure 14, a side view of the obturator 33 of Figure 13 is seen but with the spreading legs 39 and 41 in an angled apart relationship. An optional support 112 is supported by the upper control housing 37 to enable independent support and location of the obturator 33 should it be needed. Once the knurled knob 50 is turned, the wedge 51 seen in Figure 1 is driven downward causing the spreading of the spreading legs 39 and 41.

Referring to Figure 15, a sectional view taken along line 14 - 14 of Figure 12 gives a sectional view from the same perspective seen in Figure 14. Pivot blocks 59 are seen as having pivot bores 113 which enable the upper portions 53 to pivot with respect to the upper control housing 37 and which enable the downward movement of the wedge 51 to translate into a spreading of the spreading legs 39 and 41.

As can be seen, the knob 50 and control shaft 49 and the wedge 51 have the through bore 111. In the configuration shown, the control shaft 49 includes a threaded portion 114 which engaged an internally threaded portion 115 of an internal bore 117 of the upper control housing 37. The boss 47 is shown to be part of a larger insert fitting within a larger fitted bore 119 within the upper control housing 37. This configuration pushes the wedge 51 downwardly against an internal wedge conforming space 123 to cause the insertion tangs 55 and upper portions 53 to spread apart. The wedge conforming space 123 need not be completely wedge shaped itself, but should ideally have a surface which continuously and evenly in terms of area engages the wedge 51 to give even control. Further, the wedge 51 can be configured to be rotatable with or independently rotationally stable with

respect to the control shaft 49. As can be seen, the through bore 111 continues below the internal wedge conforming space 123 as a pair of curved surfaces 125 in the upper portion 53, as well as a pair of curved surfaces 127 in the pair of spreading legs 39 and 41.

Referring to Figure 16 a view of obturator 33 similar to that of Figure 15, but turned ninety degrees along its axis is seen. In this view, the wedge 51 is seen as having a narrower dimension to lend internal stability by narrowing the bearing area of the wedge 51 action in opening the pair of spreading legs 39 and 41.

Referring to Figure 17, a closeup view of the external hinge assembly 77 seen in Figure 1 illustrates the optional use of a plug 131 to cover the exposed side of the circular protrusion 81.

Referring to Figure 18, a view taken along line 18 - 18 of Figure 11 illustrates a view which facilitates the showing of an optional skirt, including a skirt section 133 welded or otherwise attached to lower tube curved portion 65, and a skirt section 135 welded or otherwise attached to lower tube curved portion 69. The skirts sections 133 and 135 are made of thin flexible metal and interfit within a pair of accommodation slots 137 and 139, respectively.

Referring to Figure 19, a view of the lower tube curved portions 65 and 69 in a close relationship illustrates the manner in which the skirts sections 133 and 135 fit within the accommodation slots 137 and 139 when the lower tube curved portions 65 and 69 are brought together to a circular configuration.

Referring to Figure 20, a cross sectional view of a patient 151 spine 153 is shown for illustration of the general sequence of steps taken for any procedure utilizing the minimal incision maximal access system 31. There are several procedures utilizable with the minimal incision maximal access system 31. Only a first procedure will be discussed using illustrative figures. Other procedures will be discussed after minor variations on the minimal incision maximal access system

31 are given below.

Procedure I: Diskectomy and Nerve Decompression

The patient 151 is placed prone on radiolucent operating table such as a Jackson Table. The patient 151 is then prepared and draped. The operative area is prepared and localized and an imaging device is prepared. A guide pin 155 is insert through the patient's skin 157, preferably under fluoroscopic guidance. In the alternative and or in combination, the patient 151 skin can be incised with a scalpel. Other features in Figure 20 include the dural sac 159, and ruptured intervertebral disc 161.

Referring to Figure 21, a fascial incisor 169 over fits the guide pin 155 and is further inserted to cut through external and internal tissue. The fascial incisor 169 is then removed while the guide pin 155 is left in place. Next, using the obturator 33, the surgeon clears the multifidus attachment with wig-wag motion of the obturator 33 tip end. Next the obturator 33 is actuated to gently spread the multifidus muscle, and then closed.

Referring to Figure 22, next the assembled Working Tube 35 - Obturator 33 is inserted into the area previously occupied by the fascial incisor 169 and advanced to the operative level lamina and remove the obturator 33. As an alternative, and upon having difficulty, the obturator 33 could be initially inserted, followed by an overfit of the working tube 35. In another possibility, a smaller size of obturator 33 and working tube 35 or combination thereof could be initially utilized, followed by larger sizes of the same obturator 33 and working tube 35. The assembled Working Tube 35 - Obturator 33 in place is shown in Figure 22 with the working ends very near the spine. The working tube 35 may be held or stabilized in the field of view by a support 181 which may have an engagement sleeve 183 which fits onto the working tube.

Referring to Figure 23, the obturator 33 is actuated to a spread orientation, which automatically actuates the working tube 35 to a spread orientation. Spread is had to the desired

exposure size. The obturator 33 is thin actuated to a closed or non-spreading position. The obturator and working tube is then again advanced to dock on the spine. The working tube 35 is then fixed to assume an open position either by utilization of the locking pin 87 or other fixation device to cause the working tube 35 to remain open. Then, once the working tube 35 is locked into an open position, the obturator 33 is actuated to a closed or non-spread position and gently removed from the working tube 35.

Referring to Figure 24, the working tube 35 is in place. The working tube 35 may be secured by structure ultimately attached to an operating table. As can be seen, the operative field adjacent the spine area is expended even though the incision area is limited. The deeper a given size of working tube 35 is inserted, the smaller its entrance area. After the working tube 35 is stabilized, the surgeon will typically clear the remaining multifidus remnant at the working level and then set up and insert an endoscope or use operating microscope or loupes. The surgeon is now ready to proceed with laminotomy.

Referring to Figure 25, further detail on the support 181 and engagement sleeve 183 is shown. A base support 185 may support a ball joint 187, which may in turn support the support 181. The support 181 is shown as supporting a variation on the engagement sleeve 183 as a pivot point support engagement end 188 having arm supports 189 and 191. The arm supports 189 and 191 engage the external pivot structure on the working tube 35 which was shown, for example, in Figure 1 to be the external hinge assembly 77.

As a further possibility, the upper angled curved portions 67 and 71 are shown as being engaged about their outer periphery by an adjustable clamp 195. Adjustable clamp 195 includes a band 197 encircling the upper angled curved portions 67 and 71. The ends of band 197 form a pair of opposing plates 199 and are engaged by a nut 201 and bolt 203 assembly.

Referring to Figure 26, a side view of the assembly seen in Figure 25 is seen with the adjustable clamp 195 operable to hold the working tube 35 open at any position. Referring to

Figure 27, a top view looking down upon the adjustable clamp 195 seen in Figures 25-27 shows the orientation of the working tube 35 and adjustable clamp 195 in fully closed position. When used in conjunction with the adjustable clamp 195, the Reinforced wear plates 73 and 93 are eliminated so as to provide a smooth interface against the exterior of the upper angled curved portions 67 and 71.

Referring to Figure 28, a variation on the obturator 33 is seen. An obturator 215 has handles 217 and 219 which operate about a pivot point 221. A working tube 222 is somewhat simplified but is equivalent to the working tube 35 and is shown as including upper angled curved portions 67 and 71. Handle 219 has a ratchet member 223 extending from it and a latch 227 pivotally connected about pivot point 229 to handle 217.

Referring to Figure 29, a variation on obturator 33 is seen as an obturator 241 having an upper housing 243, control shaft 245 having a threaded section 247 and operating through a ball nut 249. A wedge 251 is extendable down through an operation space made up of a half space 253 in a leg 255 and a half space 257 in a leg 259. Hinge structures 261 are shown attaching the legs 255 and 259 to the upper housing 243. A through bore 111 is also seen as extending from the knob 261 through to the bottom of the wedge 251. An access groove 263 is carried by the leg 259 while An access groove 263 is carried by the leg 259 while an access groove 265 is carried by the leg 255.

Referring to Figure 30, a sectional view taken along line 30 - 30 of Figure 29 illustrates the use of a central support block 271 to support the a central threaded surface 273 and the legs 255 and 259.

Referring to Figure 31, a view of a thin, inset hinge 281 utilizable with any of the obturators, but particularly obturators 33 and 241, is shown. In the case of obturator 33, by way of example, upper portions 53 accommodate control shaft 49 with its through bore 111. Inset hinge 281 may be have an inset 283 and secured with machine screws 285. Inset hinge 281

may be made of a "living hinge" material such as a hard plastic, or it can have its operations base upon control bending of a pre-specified length of steel, since the angle of bend is slight. The connection between the upper portions 53 and the upper control housing 37 may be by any sort of interlocking mechanism, the aforementioned pivot blocks 59 or other mechanism.

Referring to Figure 32, a sectional view of the obturator 33 within the working tube 35 is seen. The wedge 51 is seen at the bottom of the internal wedge conforming space 123. Once the spreading of the working tube 35 is accomplished the working tube 35 is kept open by any of the methods disclosed herein. Also seen is a pivot ball 116 to allow the control shaft 49 to turn with respect to the wedge. The pivot ball will continue to support a central aperture bore 111. Once the working tube 35 is stabilized in its open position, the obturator 33 is returned to its collapsed state as is shown in Figure 33.

Provision of electro-mechanical power to the operation of the working tube 35 can provide a surgeon an additional degree of instant control. Referring to Figure 34, a top and schematic view of the use of a remote power control to provide instant control of the working tube 25, similar to the view seen in Figure 25 illustrates the use of a remote annular control cable 301 using an internal cable 303 which is closely attached using a guide 305 and which emerges from the guide 305 and circles the upper angled curved portion 67 and 71, terminating at an end fitting 307.

The annular cable 301 is controlled by a BATTERY MOTOR BOX 311 having a forward and reverse switch 313 (with off or non actuation being the middle position). This enables the surgeon to expand the surgical field as needed and to collapse the surgical field to focus on certain working areas. BATTERY MOTOR BOX 311 is configured with gears to cause the cable 303 to forcibly move axially within the annular cable 301 to transmit mechanical power to the working tube 35.

Referring to Figure 35, a view taken along line 35 - 35 of Figure 34 illustrates how the cable 303 is held in place and a

closeup of the end termination 307.

Referring to Figure 36, a mechanically operated version of the nut 201 and bolt 203 constriction band seen in Figure 25. The mechanical power linkage can be provided remotely as by a rotating annular cable, but the basic mechanical setup shown illustrates the mechanical principles. On the bolt 203, a gear head 325 is placed, either by attachment or by the provision of a threaded member and gear head made together. A second gear head 327 is utilized to show the possibility of providing a right angle power take-off in the event that the power connection interferes with the area around the surgical field. A shaft 329 extends from a BATTERY MOTOR BOX 331. The BATTERY MOTOR BOX 331 has a forward and reverse switch 333, (with off or non actuation being the middle position). Shaft 329 could be flexible and connected directly into axial alignment with the threaded member of bolt 201 or an integrally formed threaded member.

Advantages Over Existing Surgical Techniques

In terms of general advantages, there are differences between the minimal incision maximal access system 31, and its components as described in all of the drawings herein (but which will be referred throughout herein simply as the minimal incision maximal access system 31, or simply system 31) and other devices and procedures.

1. With regard to the Traditional microdiskectomy technique, the minimal incision maximal access system 31 allows for at least the same, if not better visualization access of the operative field. System 31 offers the same 3-Dimensional work ability or, if preferred, an endoscope can be utilized. System 31 minimizes muscle injury with spread versus extensive cautery dissection. System 31 has clear advantage on the challenging obese and very large patient where the traditional microdiskectomy technique is almost impossible to be applied.
2. With regard to open pedicle screw insertion procedures, system 31 offers muscle approach minimizing muscle devascularization and denervation. The traditional approach had required at least one level proximal and one level distal

additional exposure causing extensive muscle injury often leading to "fibrotic" muscle changes resulting in chronic painful and stiff lower back syndrome. System 31 offers the most direct approach to the pedicle entry point selecting the avascular plane between the longissimus and multifidus muscles.

3. With regard to the Sextant Procedure, system 31 offers clear advantage over the Sextant procedure. First, the system 31 offers a procedure which is not a blind pedicle screw technique. System 31 can be applied to larger and more obese patients in which the Sextant procedure cannot be utilized. In this procedure using system 31 oosterolateral fusion can be performed along with insertion of the pedicle screws. The sextant procedure is strictly a tension band stabilization.

In general, the components of the minimal incision maximal access system 31 are very simple the hemispherical shapes used for the working tube can be round or oval. A keying system can be had to align the obturator 33 to the working tube 35. In the case of an oval system, the alignment would be automatic.

The minimal incision maximal access system 31 is a modular system with interchangeable parts for both the working tube 35 and the obturator 33. The guide Pin 155 is of simple construction, as is the fascial incisor 169. The working tube 35 has a limited number of basic parts, and can be made in the simple, two main piece version of Figure 28, or the multi-piece version of Figure 1, which enables retractor-sleeve substitution. A hinge and stabilization mechanism completes the simplified construction.

The obturator 33 is also of simple construction, with upper control housing 37, pair of spreading legs 39 and 41, and an internal hinge, whether the pivot blocks 59 or hinge 281 and its ability to support a control shaft 49 having a bore 111 for a guide pin 155. Guide pin 155 may preferably have a size of from about 0.3 mm to 0.40 mm diameter and 30 cm to 40 cm in length. The fascial incisor may preferably be cannulated for usage with the guide pin 155 and have a width of about 2 mm more than the associated retractor. The overall cutting head length of about 1.2 cm has a shape as indicated in the Figures

and has a thickness slightly larger than that of the guide pin 155.

The working tube 35 can have several variations and added details including the simplest shapes as dictated by intended usage. Working tube 35 can have a simple fluted hemi-tube shape or a Slanted box shape. Further, the possibility of a fluted oval shape is dictated when the approach is more angular. The working tube 35 can have an attachment for an endoscope. Working tube 35 can also have a non-symmetric appearance as by having longitudinal cross sectional shape with half of its shape being rounded and one half of its shape being rectangular or box shaped. This could also give rise to a similarly shaped obturator 33. The working tube 35 should have an anti-reflective inner coating and may be of modular construction.

The preferred lower dimensions for the lower tube curved portions 65 and 69 include an overall shape which is semi tubular round or oval and having a width of from about 1.6 - 3.0 cm and a length of from about 4.0 - 18 cm. Curved portions 65 and 69 may have custom cut outs depending upon planned application.

The hinge assembly 77 may have male-female post or male-female dial lock design, as well as a hinge housing and a bias (by spring or other mechanism) to keep angular displaceable portions of the working tube 35 closed. a "universal" port provides a point of attachment of an endoscopic or stabilizer bar.

The obturator 33 may be any controlled opening device including a circular band or cable, force Plates, or a device attached to hinge assembly 77 or other hinge assembly.

All sleeve attachments including the attachable legs 39 and 41, as well as the lower tube curved portions 65 and 69 should be of the friction grip type or snap and lock type or other suitable connection method or structure.

Obturator 215 may have squeeze grip scissor style handles 219 and 217 and a controlled dilator. It may utilize an enclosed design with a handle cover having a no-slip surface.

It may be attached to the hinge housing of the working tube or separate hinge housing. In fact, it may be of a design to be held in place solely by the working tube 35. Ideally a cavity will be provided through the center axis to contain the shaft for the dilator mechanism if applicable.

The central bore 111 of the obturator 33 may have a diameter of from about 5 - 10 mm, depending upon the size of the obturator 33 utilized. Obturator 33 should be provided in various widths and length to match working tube. The working tips of the spreading legs 39 and 41 may be changeable according to surgical procedures as described in the operative procedures herein. It may have an inner chamber, or internal wedge conforming space 123 slanted in shape wider proximal and more narrow distal to accommodate the wedge 51. The internal wedge conforming space 123 can be enclosed with expanding, contracting sleeve.

Other Procedures

Many other procedures can be facilitated with the use of the inventive minimal incision maximal access system 31 and methods practiced therewith. Procedure I, a diskectomy and nerve decompression procedure was described above with reference to the Figures. Other procedures are as follows:

Procedure II: Facet Fusion

1. Patient prone on Jackson Table with normal lordosis preserved. This can be increased by placing additional thigh and chest support to increase lumbar lordosis.
2. Insert percutaneous special guide pin perpendicular to the floor at a point 1 cm caudal to the Alar-Superior facet notch.
3. Apply a flag guide to a first guide pin 155 #1.
4. Measure skin to bone depth from the scale on guide pin 155 #1.
5. Slide drill guide mechanism on the flag guide to match the skin bone distance.
6. Insert guide pin 155 #2 through the drill guide to

dock on the superior facet.

7. Make a small skin incision for the obturator 33.
8. Working tube 35 should be small oval or round with medial cutout to maximally medialize the working tube 35.
9. Advance the working tube 35 to the L5-S1 joint and dock.
10. Drill the guide pin across the joint medial to lateral, rostral to caudal. If in proper position, advance across the joint to engage the ala.
11. Drill across the joint with a cannulated drill.
12. Check depth flouroscopically and measure.
13. Pick appropriate screw length.
14. Insert specially designed facet screw and protective bracket, secure tightly.

Procedure III: Posterior Lumbar Interbody Fusion (PLIF)

1. First half of the procedure similar to microdiskectomy (Procedure I) except for the use of a larger diameter sized working tube 35. Use a 20-25 mm round or elliptical diameter working tube 35 with a medial cutout to allow docking as close to midline as possible.

2. Following diskectomy enlarge the laminotomy to accommodate the tools use for the specific PLIF such as Brantigan cage or Tangent.

Procedure IV: Transfacet Interbody Fusion (TFIF)

1. Follow the same procedure as the PLIF in terms of selecting and inserting the Working Tube 35.
2. Following the diskectomy, resect the facet joint.
3. Approach the posterolateral disc space through the medial $\frac{2}{3}$ of the facet joint. Take care not to injure the exiting root above.
4. Proceed with Brantigan cage instruments and interbody cages.

Procedure V: Pedicle Screw Instrumentation Technique

1. Place the patient 151 Prone position on a Jackson Table.
2. Guide pin 155 is docked on facet joint angled 30 degree lateral to medial in the plane between the longissimus muscle longitudinally and multifidus muscle medially.
3. Make skin incision.
4. Fascial incisor introduction.
5. Introduce the obturator 33 working tube 35 assembly between the longissimus and multifidus and progressively open the obturator 33 tip ends of the legs 39 and 41, gradually reaching from the joint above and the joint below.
6. Advance the working tube 35 and retract the obturator 33.
7. Use the elliptical Working Tube size 2.5 cm wide and open up to 5 cm.

Procedure IV: Anterior Lateral Lumbar Diskectomy Fusion

1. Mid lateral decubitus position left side up. Place a "waist roll" to prevent sag of the mid lumbar spine.
2. Identify proper level of surgery fluoroscopically.
3. Insert a guide pin 155 #1 percutaneously into the superior facet perpendicular to the spine.
4. Measure depth skin to joint on the scaled guide pin 155 #1.
5. Insert cannulated flag guide over guide pin 155 #1.
6. Slide the drill guide to match the depth.
7. Insert a guide pin 155 #2 down to the disc space.
8. Make skin incision and insert fascial cover.
9. Insert the working tube 35 and Obturator 33 combination.
10. Progressively dilate the obturator 33.
11. Advance the working tube 35.
12. Perform anterolateral diskectomy and interbody fusion as taught above.

13. Use a round or oval shaped retractor or lower tube curved portion 65 and 69 as inserts preferably with distal end cutouts in each.

Procedure VII: Posterior Cervical Foramenotomy and Lateral Mass Plating

1. The patient is placed in a prone position on a Jackson table.
2. Fluoroscopic identification of the level of surgery is had.
3. Percutaneously insert guide pin 155 with AP and lateral fluoroscopic views.
4. Make the initial skin incision.
5. Apply the working tube 35 with obturator 33 into the incision.
6. Perform slow dilation of the muscle.
7. Advance the working tube 35 and collapse and remove the obturator 33.
8. Proceed with surgery. Type of sleeve or lower tube curved portion 65 should be round or oval with slanted and to match the slanted lamina.
9. For application for Lateral mass plating use an oval working tube 35 for a greater exposure.

Procedure VIII: Anterior Cervical Discectomy Fusion

1. Begin with standard anterior cervical discectomy fusion approach with a incision on the left or right side of the neck.
2. Blunt finger dissection is performed between the lateral vascular structures and the medial strap muscle and visceral structures down to the prevertebral fascia.
3. Establish the correct level to be operated on fluoroscopically and the guide pin 155 inserted into the disc.
4. Apply the working tube 35 and obturator 33 combination and dock at the proper level of the anterior

spring.

5. Open the working tube 35 and obturator 33.
6. Mobilize longus colli muscle.
7. Use special Bent Homen Retractor specifically design to retract the longus colli.
8. Proceed with surgery.

Procedure IX: Anterior Lumbar Interbody Fusion

1. Begin with the standard approach whether it is retroperitoneal, transperitoneal or laparoscopic.

2. Apply the special anterior lumbar interbody fusion working tube 35 and obturator 33. This is a design with a medial lateral opening. It is oval shape and preferably with skirts 133 and 135. The distal end of the retractor blade is slightly flared outward to retract the vessels safely. There is a skirt 133 or 135 applied to the cephalad side and possibly to the caudal side.

3. With the vessels and the abdominal contents safely retracted out of harms way, proceed with diskectomy and fusion.

One of the aspects emphasized up to this point for the system 31 is structure and circumstance to minimize the upper entry point of the surgery while providing an expanded working area at the distal end of the tube. Structures which achieve this geometry have been shown, and include a flared upper end so that the aperture remains open regardless of the angle of spread.

In other applications it is permissible to expand the aperture opening at the top of the working sleeve assembly. Expansion can be for the purposes of introducing further working devices into the working tube, as well as to expand and protect the visual field. For example, further working devices may include implant tools and their held implants, tools to insert plates and screws, and tools to manipulate all of these into their final positions.

Visual field protection can be introduced where the

surrounding tissue may tend to flow, move or obstruct the surgical working field. Where the bottom-most portions of the spread apart curved tube are spread apart, tissue tends to enter the space between the bottom parts of the tube. Additional guarding structure needs to be introduced.

A description of the desired articulation of what is hereinafter referred to as a working tube assembly 417, and including the working tube curved portions is begun with respect to Figure 37. The designation of working tube assembly 417 refers to all of the tube structures seen in the earlier Figures 1 - 36 and as seen in any of the following Figures.

Figure 37 is an isolated view of two curved tube sections shown joined in a tubular relationship and indicating at least a pair of pivot axes on each curved tube section.

At the top of the structure shown in Figure 37 a dashed line indicates an optional fluted structure 419. Fluted structure is omitted from the drawings for Figures 37 - 49 in order that the views from the top will not be obscured. The optional fluted opening 419 and is often employed both to maintain the visual field upon opening, as well as to make it easier to add instrumentation into the surgical field. This structure is recommended, as well as all reasonable accommodation to facilitate its use.

a first curved tube 421 is shown in alignment with a second curved tube 423. Rather than having the upper ends flared out to maintain a circular visual field on a full open position, a clearance notch 425 is provided in first curved tube 421, while a clearance notch 427 is provided in second curved tube 423.

The lowermost extent of the clearance notches 425 and 427 coincide with an upper pivot axis 431 of first curved tube 421 and upper pivot axis 433 of first curved tube 421. The pivot axes 431 and 433 may include supports either derived from structures going into or out of the first and second curved tubes 421 and 423. In the view of Figures 37 - 39, the structures seen facing the viewer are repeated on the opposite side. Thus, pivot axes 431 and 433 are also located on the

side opposite that seen in Figures 37 - 39. The same is true for all of the numbered structures. In this position, the simultaneous pivoting about the pivot axes 431 and 433 of the first and second curved tubes 421 and 423 will not cause interference by portions of the first and second curved tubes 421 and 423 which would otherwise interfere.

Further, a lower pivot axis 435 is provided below the upper pivot axis 431 of first curved tube 421. Similarly, a lower pivot axis 437 is provided below the upper pivot axis 433 of second curved tube 423. Pivot axes 441, 433, 435 and 437 may also be expected to translate. The geometry and pivot points having been identified, double headed arrows illustrate that the pivot points should be able to move toward and away from each other. Ideally, the only limitation should be the interference from the lower ends of the first and second curved tubes 421 and 423 with each other. Where the mechanism for moving the first and second curved tubes 421 and 423 has maximum independence, secondary considerations of interference are eliminated and only the primary interference between the first and second curved tubes 421 and 423 will remain. Where the control mechanism for movement is lesser than that which allows maximum independence, savings can be had in terms of complexity of the mechanism at the expense of the freedom of movement.

Figure 37 illustrates the first and second curved tubes 421 and 423 in a closely aligned relationship where the upper pivot axis 431 is closest to the upper pivot axis 433 and where the lower pivot axis 435 is closest to the lower pivot axis 437. This is the position expected to be used for entry into the body of the patient, especially along with a guide (to be shown) which will be located within and extending below the assembled and parallel linear tube formed by first and second curved tubes 421 and 423 to provide a reduced insertion resistance.

Ideally, the first and second curved tubes 421 and 423 will be inserted as shown in Figure 37 and then manipulated to a position shown in Figure 38. Figure 38 is an isolated view

of two curved tube sections as seen in Figure 38 which are angularly displaced apart about a shared first pivot axis on each of the curved tube sections. The position in Figure 38 is characterized by the fact that upper pivot axes 431 and 433 have the same separation as seen in Figure 37, but in which the lower pivot axes 435 and 437 have moved apart. The position seen in Figure 38 will be likely achieved just after insertion and in which the internal tissues have been pushed apart. Depending upon the surgical procedure, the first and second curved tubes 421 and 423 will be chosen based upon length, so that the lower end will be at the correct height for the tissues to be viewed, manipulated and treated. The action can continue until the lower ends of the first and second curved tubes 421 and 423 are sufficiently spaced apart for view and manipulation of the tissues between and adjacent the lower ends. If there is a sufficient viewing opening based upon the original distance of separation of the upper pivot axes 431 and 433, the procedure may continue through an aperture about the same size of the tube shape seen in Figure 37.

Where more of an opening is needed, the first and second curved tubes 421 and 423 upper pivot axes 431 and 433 can move more widely apart until a position such as that seen in Figure 39 is achieved. Figure 39 is an isolated view of the two first and second curved tubes 421 and 423 which are angularly displaced apart about a shared second pivot axis on each of the curved tube sections. It should be emphasized that the position seen in Figure 39 is a position where both the first and second curved tubes 421 and 423 are parallel and separated from each other, but this need not be the case. From the position seen in Figure 38, the upper pivot axes 431 and 433 can be moved apart from each other while the lower pivot axes 435 and 437 either remain a constant distance from each other or are brought together. This range of articulation described can be used to physically manipulates the tissues in contact with the first and second curved tubes 421 and 423 for any number of reasons, including introduction of further instruments if necessary, as well as to react to changing

conditions of tissue at the lower tube.

In both Figures 38 and 39 a pair of opposing edges 439 can be utilized to support structures introduced between the first and second curved tubes 421 and 423. Other structures can be used including depressions, apertures and internal projections, such as hooks or latches. An internal structure within the first and second curved tubes 421 and 423 would pose little risk of nick to the patient and can be designed to do nothing more than have a minimal interference effect with respect to the visual field.

As will be shown, a number of external structures can be employed to achieve the relative separation positions of the upper pivot axes 431 and 433, as well as the lower pivot axes 435 and 437 that nearly any type of angle can exist on either side of a parallel relationship between the first and second curved tubes 421 and 423, but that most will be in a range of from a parallel relationship to some form of angular relationship seen in Figure 38, where the upper ends at the clearance notches 425 and 427 are closer together than the lower ends distal to the upper pivot axes 431 and 433 and lower pivot axes 435 and 437.

One example of a side shield 441 is seen in Figure 40. Figure 40 is a plan view of a given width supplemental side shield 441 having a width of approximately the separation of the curved tube sections as seen in Figure 39, while accompanying Figure 41 is a top view of the supplemental side shield 441 of Figure 40 emphasizing its shape. The side shield 441 can be of any shape, but is shown in a rectangular shape to correspond with the first and second curved tubes 421 and 423 in a parallel position as seen in Figure 39. The side shield 441 has a main portion which includes a first side 443 and a pair of lateral engagement portions 445. The side shield 441 can depend from a number of other structures, but the side shield 441 seen in Figures 40 and 41 utilize an offset surfaces as engagement portions 445. This geometry, will, absent any interfering structures which are attached to manipulate the first and second curved tubes 421 and 423, enable the side

shield 441 to be introduced linearly from the top of first and second curved tubes 421 and 423. The introduction of side shield 441 may be guided somewhat into engagement by the clearance notches 425 and 427. Much smaller engagement portions 445 could be used to engage the outer edges 439 of the first and second curved tubes 421 and 423, so long as the orientation is so as to protect the surrounding tissues. Figure 41 emphasizes the geometry and shows a second side 447.

In the orientation shown, the second side 447 would face toward the inside of the general tube formed in the orientation of Figure 39. If two of the side shields 441 were used, one on either side of the opening seen in Figure 39, the tube shape would be closed on both sides, and an oval viewing area would be formed. It should be emphasized that the side shield 441 can depend from any structure, and not just the opposing edges 439 seen in Figure 39. Structure used to manipulate the first and second curved tubes 421 and 423 can be used to both guide and secure any side shield 443.

In terms of a structure to manipulate the first and second curved tubes 421 and 423, it is preferable that the upper pivot axes 431 and 433 may be urged toward and away from each other independently of the urging of the lower pivot axes 435 and 437 toward and away from each other independently. a mechanism which would prevent all manipulations of the first and second curved tubes 421 and 423 to a position of binding is desirable, but its complexity may obstruct the surgical field. For example, it would be good to have a mechanism which would prevent upper pivot axes 431 and 433 from moving away from each other while the lower pivot axes 425 and 437 are in their close proximity as depicted in Figure 37. In some cases operator knowledge and skill will probably be required.

In terms of supporting the upper pivot axes 431 and 433 and lower pivot axes 425 and 437, the pivoting and movement may be passive with mechanisms to push or pull directly on the first and second curved tubes 421 and 423 or structures which are mechanically attached. As an example of the use of force and movement urging at the pivot points, Figure 42 illustrates

one such system as a pivoting thread support system 551. The gearing is shown as unduly expansive to illustrate simply the action, but in reality, several gears may be used.

Further, since the a pivoting thread support system 551 is viewed from the top, and as operating the upper pivot axes 431 and 433, a similar arrangement would be used for the lower pivot axes 425 and 437. a set of four pivot fittings 553 provide a threaded interior spaced apart from the first and second curved tubes 421 and 423, or fittings supporting the first and second curved tubes 421 and 423. The fittings 553 enable the first and second curved tubes 421 and 423 to tilt while keeping the threaded apertures in alignment.

a first threaded member 555 has a pair of threaded areas in which the threads are oppose pitched. The threads engaging the fitting 553 of first curved tube 421 are set to urge first curved tube 421 away from second curved tube 423, at the same time that the same turning of the first threaded member engages fitting 553 of first curved tube 423 set to urge first curved tube 423 away from second curved tube 421. This means that the turning of first threaded member 555 in one direction urges the first and second curved tubes 421 and 423 evenly away from each other, and alternatively, the turning of first threaded member 555 in the opposite direction urges the first and second curved tubes 421 and 423 evenly toward each other.

Likewise, a second threaded member 557 has a pair of threaded areas in which the threads are oppose pitched. The threads engaging the fitting 553 of first curved tube 421 are set to urge first curved tube 421 away from second curved tube 423, at the same time that the same turning of the first threaded member engages fitting 553 of first curved tube 423 set to urge first curved tube 423 away from second curved tube 421, but in an oppose orientation than the threads of first threaded member 555. This means that the turning of second threaded member 557 in the other direction (while the first threaded member 555 is turned in a first direction) urges the first and second curved tubes 421 and 423 evenly away from each other. a pair of over sized gears, including a first gear 559

associated with the first threaded member 555, and a second gear 561 associated with the second threaded member 557 act to cause the first and second threaded members 555 and 557 to move simultaneously and oppositely. a knob 563 is used to manipulate both the first gear 559, which manipulates the second gear 561. In a realization in which more gears 559 and 561 are provided, the size of the gears can be reduced and for each intermediate gear, the sense of the threaded members 555 and 557 will change from opposite to same.

Referring to Figures 43 and 44, a surrounding frame system 571 is seen which is utilized to provide and enable pivoting and translation. A surrounding frame 573 has an open slot 575 which accommodates a pair of pins 577 and 579 which preferably have some tracking along the slot 575 to insure that neither the first curved tube 421 nor the second curved tube 423 are able to turn within the frame 573. The opposite side of the frame 573 will have a similar slot 575. However, where the structures which engage the slot are especially over sized, or where the structural integrity is sufficient, only one slot need be used. The structural dependence on the frame 573 should be such that the two opposing first and second curved tubes 421 and 423 will always oppose each other and cannot twist away from each other and can only pivot along their long axis.

a turn fitting 581 enables a threaded member 583 to turn while being axially fixed to the first curved tube 421. The threaded member 583 may be threadably engaged to an internal thread 585 at the end of the frame 573. In this case a knob 587 is used to manually turn the threaded member 583 independently to move the first curved tube 421 to the left or to the right. A turn fitting is a structure which holds the end of the threaded member and allows the threaded member 583 to urge the fitting forward or backward while continuing to turn.

In the alternative, knob 587 may have an internal thread, and turned with respect to the threaded member 583 draw the threaded member out of the frame 573. In this case, a spring

(as will be shown) could be used to help reverse this operation. Where the knob 587 is internally threaded, the end of the threaded member may be fixed directly to its first curved tube 421.

In sum, there are three ways to affect motion, preferably the internal threads 585 enable the threaded member 583 to turn to urge first curved tube 421 in both directions with respect to the frame 573. In the alternative, the threaded member 583 may act only to urge the first curved tube 421, and the tubes 421 and 423 may have another mechanism urging them apart or simply move apart based upon other forces or other structures present. Third, the threaded member 583 may have an end anchored to the first curved tube 421 with an internally threaded surface inside knob 587 to enable the knob 587 to be turned to cause the length of threaded member 583 to be withdrawn from the frame 583. A spring, or other fitting can be used to help reverse the direction of travel. All of the knobs and threaded members shown hereafter have the ability for all three modes of action.

Similarly, a turn fitting 591 enables a threaded member 593 to turn while being axially fixed to the second curved tube 423. The threaded member 593 threadably engaged to an internal thread 595 at the end of the frame 573. a knob 597 is used to manually turn the threaded member 593 independently to move the second curved tube 423 to the left or to the right.

Similarly, a second surrounding frame 573 has an open slot 575 which accommodates a pair of pins 601 and 603 having expanded heads which fit outside the slot 575 to provide tracking along the slot 575 to further insure that neither the first curved tube 421 nor the second curved tube 423 are able to turn within either of the frames 573.

a turn fitting 611 enables a threaded member 613 to turn while being axially fixed to the first curved tube 421. The threaded member 613 is threadably engaged to an internal thread 615 at the end of the frame 573. a knob 617 is used to manually turn the threaded member 613 independently to move the first curved tube 421, at its lower pivot axis 435 at the

center of the pin 601. Similarly, a turn fitting 621 enables a threaded member 623 to turn while being axially fixed to the second curved tube 423. The threaded member 623 threadably engaged to an internal thread 625 at the end of the lower located frame 573. a knob 627 is used to manually turn the threaded member 623 independently to move the second curved tube 423 to the left or to the right at its lower pivot axis 437 at the center of the pin 603.

With the configuration of Figure 43, the position within the upper located frame 573 and separation of the pivot axes 431 and 433 (represented by the pins 577 and 589) can be exactly specified. Likewise, the position within the lower located frame 573 and separation of the pivot axes 435 and 437 (represented by the pins 601 and 603) can be exactly specified. In typical use, the knobs 617 and 627 and will be activated after insertion to achieve the configuration seen in Figure 38, and then followed by the use of the knobs 587 and 597 to achieve the configuration seen in Figure 39, if necessary. Thereupon the optional side shield 441 may be employed. Where a lesser separation than that seen in Figure 39 is used, a narrower side shield 441 may be employed. In a surgical kit, several such shields 441 of different size and shape may be available.

Referring to Figure 44, a view looking down into the structure of Figure 43 shows the overall orientation and further illustrates an optional securing tang 629 which may be used with either of the upper located or lower located frame 573, and may be located in any position, or extended in any direction, to better enable the surgeon to stabilize and manipulate any of the assemblies 417, 551 and 571 seen. Any structure can be used to help secure the frame 573 and or the first and second curved tubes 421 and 423. Figure 44 is an equivalent view through the lower of the frames 573, including the knobs 617 and 627 as the two frames 573 have equivalent action. Note that having complete control over both the separation, angular relationship, and position of the first and second curved tubes 421 and 423 within the frame 573 will

enable the surgical practitioner to position the line of sight of the working tube along the frame 573 length and to generally have complete control.

Also shown in Figure 44 is an optional spring 630 which can be used to bias the force acting upon either of the first and second curved tubes 421 and 423, or it can be used to bias a knob 597 away from the frame 573. Although shown as an option, the use of a spring 639 may contribute significantly where force is to be had in one direction only, as well as to lock a threaded member such as 593 into a turn fitting by keeping a pulling bias in place.

In some cases it may be desired to reduce the number of controls to accomplish certain objectives, such as simplicity, less controllability, less moving parts, inexpense, or the critical need for space about the upper part of any of the assemblies 417, 551 and 571. One example of an arrangement is seen in Figure 45. a frame 631 has an interior having one surface which may generally match one of the first and second curved tubes 421 and 423, and in this case first curved tube 421. The frame 631 may be attached to the first curved tube 421 by tack welding or the like, or other means. a single threaded member 633 includes a knob 635. a structure 637 can be either an engagement turning block to enable the threaded member 633 to both push and pull on the second curved tube 423, or it may simply be a wear block to allow the threaded member 633 to push against it and to protect the second curved tube 423 from wear.

Because half of the tube assembly of first and second curved tubes 421 and 423 is supported by the frame 631, the second curved tube 423 is left to move only slightly and assuming that Figure 45 is an upper view and that the pivoting of the second curved tube 423 is accomplished at a lower level, especially at the level of lower pivot axis 437, the frame 631 is left to control second curved tube 423 by simply pushing, or by pushing and pulling. Where structure 637 is a turning block, there is a bulbous expansion at the end of threaded member 633 which snaps into structure 637 as a turning block

and is free to turn and both push and pull second curved tube 423. The threaded member 633 is threadably engaged into an internal threaded bore 639 within the frame 631.

Referring to Figure 46, one embodiment of a manipulative structure which works well with the structure of Figure 45 is shown. The structure shown is a partial section taken at the lower pivot axis level and includes means for pushing and pulling, or pushing alone. Preferably, when used with the structure of Figure 45, it will include pushing and pulling, especially if the structure of Figure 45 performs pushing alone. Either of the structures in Figure 43 at either the upper or lower pivot axis levels can be substituted for either of the structures shown in Figure 45 and 46 as the structures in Figure 43 provide both pushing, pulling, pivoting and level support.

Where the structures of Figure 45 provides both pushing and pulling, it can be used along with a second structures at the lower pivot axis as any structure which provides both pushing and pulling will also provide some pivoting support. Further, the structure shown in Figure 46 is hinged to provide additional pivoting support. The structure of Figure 46 can be used at either the upper pivot axes 431 and 433 or the lower pivot axes 435 and 437. Both the structures of Figure 45 and 46 demonstrate clearly that lesser control structures than are shown in Figure 43 can be used to control the first and second curved tubes 421 and 423, along with lesser control inputs, and less control specificity, but also with less moving parts and a lesser mechanical complexity.

Referring again to Figure 46, second curved tube 423 is seen as tack welded to a reinforcement 651. The purpose of reinforcement 651 is to provide an expanded thickness of material so that pivoting can occur closer to the opposing edge 439 as is possible. It is further possible to continue the extent of the reinforcement 651 and its pivot point in the direction of first curved tube 421 if the other geometries of the other components permit. Reinforcement 651 contains a pair of threaded bores 653, each of which accommodates one of the

threaded screws or bolts 655 shown. The bolts 655 each extend through one end of a "U" shaped fitting 657, so that the reinforcement 651 and attached second curved tube 423 pivots with respect to the fitting 657. a threaded member 659 engaged an internal threaded bore 671, and has a knob 673 for ease of manual operation.

The threaded member is connected to a turn fitting 675 the first curved tubes 421 to be moved toward and away from second curved tube 423. The use of the structure of Figures 45 and 46 may be used together to give the ability to provide control, although not as much control as is seen in Figure 43.

Referring to Figure 47, another possible realization is seen, combining the control mechanisms of selected portions of Figures 37 - 46, combined with other possible options. An open frame system 691 is seen as having a frame 693 which is either open on at least one side, or which has a side expanded to a distance sufficient to introduce other structures to expand in that direction. Some of the components previously seen include pins 577 and 579 extending through slot 575. Pins 577 and 579 may have extended vertical and horizontal extent to garner additional stability from the frame 693, especially where one side is open.

Other structures may be used to insure that neither the first curved tube 421 nor the second curved tube 423 are able to turn within the frame 573. Also seen are turn fitting 581, threaded member 583, knob 587, turn fitting 591, threaded member 593, and knob 597. The view of Figure 47 is from above, and thus the structures most closely correspond to the upper structures seen in Figures 43 and in Figure 44.

As can be seen in Figure 47, a four point retractor system can be formed with the components and structures of the foregoing Figures. The first and second curved tubes 421 and 423 are shown in the open position. On the longer connector arm of the frame 693, a side shield 695 is supported. The side shield 695 can derive its ability to hold tissue out of the visual field by being locked down onto the frame 693 in the same manner as a wrench fits a bolt head. In this

configuration, the side shield can be inserted into the center of the surgical field and then rotated into position and moved down slightly to lock it into place. On the opposite side from side shield 695 is a retractor 697 which has a flat portion entering the surgical field and which is controlled from a point remote with respect to open frame system 691. An angled portion 699 turns from the flat portion seen entering the surgical field and extends down into the area between the open first and second curved tubes 421 and 423.

Also seen are a series of small circular structures 701 about the peripheral upper surface of first and second curved tubes 421 and 423. These structures are at least one of embedded fiber optics and ports for accepting fiber optics. The apertures formed in the metal open at a slight angle to the inside of the first and second curved tubes 421 and 423 to direct light into the surgical field without producing a back reflection or other scatter. In cases where the fiber optic is permanently affixed, a light ring section can simply be snapped to or placed on the first and second curved tubes 421 and 423. In cases where the apertures are provided, surgery can continue without fiber optics, or a fiber optics set can be added which can range from an illuminated ring (relying on low angle of incidence and Snell's law) to direct light through the openings which open to the inside of the first and second curved tubes 421 and 423 at a low angle of incidence. Intermediary solutions, such as a light ring having a series of short fiber optic members for insertion into the apertures can be used. To facilitate the use of fiber optics, the curved tubes 421 and 423 may be made from a composite material in which the fiber optic components may be present during formation of the tube structures. Other material may be used for tubes 421 and 423, including materials that either transmit light or have portions which transmit light.

As an alternative to the three sided frame 693, the open portion of the frame could be enclosed by an expandable member 703 which can have any manner of interlock with the three sided frame 693. One such interlock is illustrated as simply an

annular piston dependence where the expandable member 703 includes a smaller tubular insert 705 which fits closely into a matching bore 707 seen in the terminal ends of the three sided frame 693. The expandable member 703 can be used to lend additional support to the three sided frame 693, especially forces produced by the threaded members 583 and 593. The expandable member 703 is also useful to help support the retractor 697 where such provision is made. The main purpose of expandable member 703 is the adjustability to give greater clearance and access. The same adjustability could be had on the side of three sided frame 693 which supports side shield 695, especially with a more complex mechanism to enable the frame expansion to be locked into place. A locking mechanism for expandable member 703 is not shown so that the drawings may be simplified, but lock ability can be achieved in the same manner as any metal to metal frame construction known in any field of art.

Referring to Figure 48, a side view of the side shield 695 is seen. The clearance for locking onto the frame 693 is about the same as the width of the frame 693 so that non rotational fixation can be transmitted along the length of the side shield 695.

Referring to Figure 49, one possible configuration is seen for a variable depth guide 711 which is utilizable with any of the devices seen in Figures 37 - 46 or any other tubular, minimally invasive system. Variable depth guide 711 has a handle 713 controlling a shaft 715. Shaft 715 has a through bore 717 which is used to insert a guide line or guide pin to help insert any minimal access system seen in the earlier Figures.

A translatable detent ring 719 interacts with a series of detent indentations 721. The position of the detent ring 719 will correspond to the lengths of the first and second curved tubes 421 and 423 with which the variable depth guide 711 is used. Once the practitioner inserts the variable depth guide 711 into any assembly containing a first and second curved tubes 421 and 423, the necessary height can be adjusted so that

the tip of the variable depth guide 711 extends just beyond the lower extent of the joined first and second curved tubes 421 and 423. The height is adjusted by forcing the detent ring 719 to the proper detent indentation 721, and then inserting it into a closely associated first and second curved tubes 421 and 423 to form an overall bullet shape for insertion, preferably a guide pin 155. Once inserted, the variable depth guide 711 is removed. The detent ring 719 carries a frusto-conical surface 723 where it is used with first and second curved tubes 421 and 423 having fluted top areas as seen in Figure 37 and in previous figures. Any mechanism can be used to achieve a detent action, including an internal pressure ring or a spring loaded bar, or protruding ball bearings. The positional stability of the detent ring can be specified by the spring action of the detent member, and should be sufficiently stable to enable deliberate manual fixation with no inadvertent movement occurring even where significant resistance is encountered.

Referring to Figure 50 is a vertical plan view looking down upon an expandable frame system 751 which uses detents to set the frame size and which uses an angular distribution system. A frame is used as a support and reference point to manipulate a working tube in much the same way as Figures 37 - 47. Expandable frame system 751 enables the user to control the size of the operating theater as needed. Where the task can be accomplished with minimum opening access, such minimum opening is all that needs to be taken. Where greater access is needed, the expandable frame system 751 provides both an expanded work space, and additional surfaces for support of other instrumentation.

As before, the retractor blades are seen as a first curved tube 753 having an upper flared portion 755 and a second curved tube 757 having an upper flared portion 759. Each of the first and second curved tubes 753 and 757 have two points of variable pivoting attachment.

Curved tube 753 has a pivot bar 781 which may be attached somewhat tangentially to the first curved tube 753, or may

include a pair of extensions attached to the outside of the first curved tube 753. Likewise, curved tube 757 has a pivot bar 783 which may be also attached somewhat tangentially to the first curved tube 753 in the same manner.

Pivot bar 781 has circular lands 785 which fit into support fittings 787. Likewise pivot bar 783 also has circular lands 785 which fit into support fittings 787. The support fittings 787, as seen from above, show the lands 785. In this configuration the lands 785 can be dropped in from above. This is an over-simplified illustration, as some other locking mechanism can be utilized, including ball shape instead of disc shape or other. It would be preferable that the manner of pivoting engagement will firstly enable an ease of assembly and disassembly and secondly provide good stability against dislodgement with respect to any forces experienced when the expandable frame system 751 is in an operational position.

Above the point of pivot of the pivot bars 781 and 783, each of the first and second curved tubes 753 and 757 are fitted with a pivot bearing fitting 791. The pivot bearing fittings 791 can depend from either the first and second curved tubes 753 and 757 or their upper flared portions 755 and 759. The pivot bearing fittings 791 can be hinge type or ball type, or any other type which will enable the upper part of the first and second curved tubes 753 and 757 to be force moved to pivot them with respect to the pivot fittings 781 and 783 in either direction.

The pivot bearing fitting 791 is engaged by a cooperating fitting 793 which enables the pivot bearing fitting 791 to pivot with respect to the cooperating fitting 793. The cooperating fitting 793 is moved with a threaded member 795, having a thumb control wheel as a tilt screw knob 797. In the drawings of Figure 50 and 51, the fittings 791 are located above the pivot bars 781 and 783, but they need not be.

In the embodiments of Figures 50 and 51 the movement of the axes of the pivot bars 783 are affected by the expansion of a frame support including a first lateral member 801 and a second lateral frame member 803. The ends of first and second

lateral members 801 and 803 are connected to two telescoping frame members 805 and 807. Telescoping frame member 805 has a central hinge box 811 which is positioned between a first sleeve 813 and a second sleeve 817. The central frame section pivotally supports a pair of internal spreading bars, including a first spreading bar 821 which extends within first sleeve 813 and a second spreading bar 823 having a ratchet or detent structure (to be described) which extends within second sleeve 817.

Although not shown in Figures 50 and 51, the spreading bars 821 and 823 will preferably have an internal gear mesh so that both will preferably have an equal angular displacement with respect to the central hinge box 811. The articulation within the central hinge box 811 will enable the selection of three angular frames of reference with regard to the surface of a patient, namely the angle of first sleeve 813, the angle of central hinge box 811, and the angle of second sleeve 817. Where other objects, such as retractors, light sources etc have to be anchored, three reference angle surfaces are available.

The spreading bars 821 and 823 are thus axially fixed with respect to the central hinge box 811, with the spreading bars 821 and 823 axially slidable within the first and second sleeves 813 and 817. Many mechanisms can be utilized to fix the position of the spreading bars 821 and 823 within the first and second sleeves 813 and 817. One such mechanism is shown schematically in its most rudimentary form in Figure 38 as including a pivot support 825 which supports a lever 827. The lever 827 operates against a spring 829 and operates an engagement member 831 with respect to detent structures 833 located on the spreading bars 823. These structures form a first ratchet stop 835. Operational depression of the lever 827 disengages the detent structures 833 of the spreading bar 823 to slide within the sleeve 817 and releasing the lever 827 enables the spring 829 to act to cause engagement of the engagement member 831. With this mechanism, or a similar mechanism, the expansion of the expandable frame system 751 can be controlled, with the expansion of the second lateral frame

member 803 away from the central hinge box 811. Similarly the first lateral member 801 is independently movable away from central hinge box 811 with the use of a mechanism similar to the one shown with respect to the pivot support 825, lever 827, spreading bar 823 engagement member 831, and detent structures 833.

The detent structures 833 could be made triangular shaped for sliding in one direction with some form of fixation hold against movement in the other direction. A second mechanism similar to the one shown with respect to the pivot support 825, lever 827, spreading bar 823 engagement member 831, and detent structures 833 is omitted from Figures 50 and 51 for simplicity. Regardless of the structure, the expandable frame system 751 can be exactly positioned. Other assisted mechanisms can be employed, including a threaded member or a pinion or other device which will give the user mechanical advantage in extending the expandable frame system 751. Further, the fittings illustrated, including pivot bars 781 & 783 with circular lands 785 and slip fitting into support fittings 787, as well as the pivot bearing fitting 791 and cooperating fitting 793 suggest that the expandable frame system 751 may be added to the operating theater after the first and second curved tubes 753 and 757 have been employed into the surgical opening. This will free the surgeon to position the first and second curved tubes 753 and 757 without having to handle the supporting frame members.

Between the other ends of the first lateral member 801 and second lateral frame member 803 the second telescoping frame member 807 also has a central hinge box 811. Again, the central hinge box 811 which is positioned between a first sleeve 813 and a second sleeve 817. The central frame section pivotally supports a pair of internal spreading bars, including the first spreading bar 821 within first sleeve 813 and the second spreading bar 823 which extends within second sleeve 817.

The interfit between the first and second sleeves 813 and 817 and the first and second spreading bars 821 and 823 in both

the first and second telescoping frame members 805 and 807 is expected to be of sufficiently tight tolerance so that both of the central hinge boxes 811 remain directly across from each other to enable a common effective pivot axis. If the latch mechanism supported by the second lateral frame member 803 is released the second lateral frame member 803 should move away from the central hinge box 811. In other words, one of the central hinge boxes 811 should not displace to a position other than directly across from each other.

The second telescoping frame member 807 could have the same mechanism as the first telescoping frame members 805, but a slightly different mechanism is shown in order to emphasize the variability which can be employed with respect to the expandable frame system 751. A retention housing 837 is attached to second sleeve 817 and houses a lock pin 839 and a spring 841 which urges it into the second sleeve 817 where it lockably interfits with the detent structures 833. These structures may be collectively referred to as a second ratchet stop 843. The expansion of the expandable frame system 751, if properly toleranced will enable the right and left sides to be independently controlled in movement toward and away from the away from the central hinge box 811. The actuation of one release mechanism will enable balanced displacement of its associated first or second lateral members 801 and 803.

Movement of the associated first or second lateral members 801 and 803 by one of the latches shown gives a parallel distance separation of the first curved tube 753 with respect to the second curved tube 757, regardless of their respective angular positions (assuming no interference). However, the angularity of the first and second curved tube 753 and 757 are set by the movement of the threaded member 795. As such, the expandable frame system 751 enables independent angularity adjustment for the first and second curved tube 753 and 757 and independent parallel separation for the first and second curved tube 753 and 757 based upon expansion of the frame.

Other features seen in Figures 50 and 51 include a support tang 845 and a pair of manipulation sphere projections as

spreader projections 847 to assist in manually manipulating the expandable frame system 751. Figure 51 illustrates a condition in which the expandable frame system 751 is in an expanded orientation, with first lateral member 801 and second lateral frame member 803 equally expanded from central hinge box 811. Either of the first and second lateral members 801 and 803 could have been extended from the central hinge box 811. This feature gives the surgeon the flexibility to adjust the positioning of the central hinge box 811. The central hinge box 811 may also have support structures for other instrumentation, including bores 849 in the central hinge box 811 such as a bookwalter support (to be shown). Bores 849 can be used for locational registry or for threaded attachment. A bookwalter device is especially useful for supporting an additional retractor, in addition to the first and second curved tubes 753 and 755.

Referring to Figure 52, a side view of the system of Figures 50-51 illustrates further details. The angle of the incline of the upper flared portions 755 and 759 are illustrated. A scale 851 helps the surgeon to ascertain the depth to which the first and second curved tubes 753 and 755 are inserted into the patient (with the additional consideration of any further extension which may be added to the first and second curved tubes 753 and 755).

One possible configuration for the first and second curved tubes 753 and 755, include the use of an upper tube portions along with a lower extension. The scale 851 could also be utilized, in conjunction with the extension to indicate depth. A notch 853 in each of the first and second curved tubes 753 and 755 can be used as a reference surface to engage an extension. Another surface can include a raised portion or depressed portion matched to an extension (as will be shown) in each of the first and second curved tubes 753 and 755.

Figure 53 illustrates a double pivot hinge fitting within the central hinge box 811. A pair of threaded members 861 extend into machined spaces within central hinge box 811 and hold the spreading bars 821 and 823 into a close proximate

location such that the complementary gear teeth 863 located on the abutting ends of the spreading bars 821 and 823 intermesh with each other. This arrangement insures that the angular displacement of the spreading bars 821 and 823 with respect to the central hinge box 811 will be equi-angular. This is shown in Figure 54 where the angle γ on both sides indicates equi angular displacement.

Referring to Figure 55, a top view of the central hinge box 811 illustrates a bookwalter retractor device 871 mounted on the upper surface of the central hinge box 811. The bookwalter device has a central through bore 873 through which a retractor rail or extension may pass. Typically the retractor extension (not shown) will have a series of detents similar to the detents 833 seen in Figure 53. As the detents emerge from the through bore 873, they are engaged by a pivoting latch 875 which operates under urging force from a spring 877. A turnbuckle or other force control structure would enable operation of a gear mechanism to move any type of "east west" retractor blades towards or away from the center.

Referring to Figure 56, a plan view is shown of a remote force retraction system employing many of the structures seen in Figures 50-55, but with a remote force system such as disclosed and shown in U.S. Patent No. 4,747,394, to Robert S. Watanabe, and incorporated by reference herein. The technique of application of remote force to leave the surgical field open as applied to the expandable frame system 751 is seen as an open minimally invasive expansion system 901. At the surgical field, many of the components previously seen have the same numbering.

A pinion box 903 carries a (removable) key insertable gear 905 seen inside an aperture 907 having teeth 911 which engage a linear gear 913 on a first rack 915, and which also engage linear gear 917 on a second rack 919. To enable the pinion box 903 to move independently and proportionately with regard to structures through which the rack 915 passes, rack 915 is fixedly attached to a first main support 921 while rack 919 is fixedly attached to a second main support 923. As the gear 905

is turned clockwise, the rack 915 freely feeds through an aperture 931 (seen in dashed line format) in second main support 923, through the pinion box 903 and pushes first support 921 farther away from the pinion box 903. At the same time, the gear 905 pushes the rack 919 freely feeds through an aperture 933 (seen in dashed line format) in first main support 921, through the pinion box 903 and pushes second support 923 farther away from the pinion box 903.

The result is that two strong support members, namely first support 921 and second support 923 are being forced away from each other remotely, by the turning of the key insertable gear 905. Note that the areas on either side of the first and second curved tubes 753 and 755 are clear to enable other structures to be employed, either unsupported, or independently supported, or possibly supported from structures which support first support 921 and second support 923.

A ratchet latch lever 935 is mounted is mounted to pivot with respect to first support 921 by the action of a spring 937. The ratchet latch lever 935 is fork shaped to fit around the tip fixed end of rack 914 and to actuate an internal latch 939 which operates within the first support 921 between the first rack 915 and second rack 919.

Also seen is a hinge 941 on first support 921, and a hinge 943 on second support 923. The hinges 941 and 943 should preferably have the same angular range and would ideally be from about zero degrees (flat) to about fifteen degrees down with the hinges 941 and 943 rising to form the apex. The hinges 941 and 943 permit the lateral force components to be angularly sloped down, or draped to provide an angled working presentation, and to take up less lateral space in the same plane as the working area. Beyond the hinges 941, the first support 921 is connected to a first extended support 945 while the second support 923 is connected to second extended support 947.

Both the first and second extended supports 945 and 947 include angular extensions 949 which support the support fittings 787 and other structures previously shown. The first

and second extended supports 945 and 947 also support tilt screw knob 797 and manipulation sphere projections as spreader projections 847. The support details for the first and second curved tubes 753 and 755 is essentially the same as was shown for Figures 50 & 51.

In addition, an optional pair of tilt fittings enable the first and second extended supports 945 and 947 to tilt where it may be more advantageous to locate open minimally invasive expansion system 901 over portion of a patient's body which is angled. A first tilt adjustment fitting 951 can be used to provide tilt to the main extent of first extended support 945, while a second tilt adjustment fitting 953 can be used to provide tilt to the main extent of second extended support 947. Typically the first and second tilt adjustment fittings 951 and 953 will be used to set the tilt before an operation begins. As to both of the first and second tilt adjustment fittings 951 and 953, a support plate 955 is rigidly supported by the portion of the respective first and second extended supports 945 and 947 nearest the hinges 941. The support plate 955 supports a retention housing 837. The retention housing includes a lock pin 839 and a spring 841 which urges it through apertures of the support plate 955 and across to a selector plate 957. As to both of the first and second tilt adjustment fittings 951 and 953, the selector plate 957 is rigidly supported by the portion of the respective first and second extended supports 945 and 947 on the other side of the respective first and second tilt adjustment fittings 951 and 953.

Although shown in somewhat schematic view, a tilt pin 961 joins portions of first extended support 945 rigidly while enabling the tilting of the portion of the first extended supports 945 on one side of the first tilt adjustment fitting 951 to pivot with respect to the portion of the first extended supports 945 on the other side of the first tilt adjustment fitting 951. Likewise, a tilt pin 963 joins portions of second extended support 947 rigidly while enabling the tilting of the portion of the second extended supports 947 on one side of the

second tilt adjustment fitting 953 to pivot with respect to the portion of the second extended supports 947 on the other side of the second tilt adjustment fitting 953. In reality, in order to transmit the force rigidity, more complex internal fittings may be utilized. The support plate 955 and selector plate 957 are simple mechanical mechanisms which are located far enough off the axis of pivot to enable selection of a number of angular positions.

Other structures can be supported from the both the first and second extended supports 945 and 947. A pair of slot openings 965 at the far ends of the first and second extended supports 945 and 947 can support additional instrumentation. In addition, the first and second extended supports 945 and 947 include structures 965 which may be apertures or projections or other structures which will enable support to be derived for other retractors. A cross support 971 supports a mechanical housing 973 through which a linear gear 975 can extend. A retractor 976 (which can be of any type) is attached to one end of the linear gear 975. A hand wheel 977 operates a gear 979 which moves the linear gear 975 through the housing 973. This assembly is a first cross supported retractor set 981. A second cross supported retractor set 983 is also shown. This gives the surgical practitioner good control and leverage to operate the "north-south" retractors.

An illustration of an extension previously mentioned is illustrated in Figure 57 which illustrates a top view of a curved extension 991 standing alone. Curved extension 991 may have several pair of inwardly directed members 993 (or a single large inwardly directed member 993) for engagement against the notches 853 seen in Figure 52. An inwardly directed angled "snap" protrusion 995 springs into a matching opening on either of the first and second curved tubes 753 and 755. The curved extension 991 will fit on the outside of the matching first or second curved tubes 753 and 755 and the force on the curved extension 961 is expected to be inward at its lower extent during spreading.

Referring to Figure 58, a side semi-sectional view is

shown. A lower portion of first curved tube 753 having groove 853, and a slot 997 is seen in a sectional view. Adjacent the semi section curved tube 753 is the curved extension 991 in an attached position. The upper end of the notch 853 fixes against up motion, and the slot 997 fixes against down motion when it engaged with inwardly directed angled "snap" protrusion 995. A stable support relationship is shown.

Referring to Figure 59, a view looking down into the inside of the combination of the first curved tube 753 and curved retractor tube extension 99 of Figures 57 and 58. It can be seen how the large inwardly directed members 993 wrap around the groove 853 and can be slid upwardly until the inwardly directed angled "snap" protrusion 995 engages.

Referring to Figure 60, a view looking down onto the outside of the combination of the first curved tube 753 and curved retractor tube extension 99 of Figures 57 - 59 is seen. In addition, the pivot bar 781 with circular lands 785 are also seen below the pivot bearing fitting 791, for reference. The large inwardly directed member 993 is partially shown in dashed line format. The bottom of the curved extension 991 may be of any shape.

Referring to Figure 61, an exploded view of a frame retractor system 1001 is seen. The articulation of the frame retractor system 1001 is achieved by using a main outer first frame section 1003 which laterally overlaps a smaller laterally inner second frame section 1005. The frame sections 1003 and 1005 are joined and circumferentially envelop a first retractor member 1007 and a second retractor member 1009. As seen in the earlier embodiments, each degree of motion achieved in retraction, namely separation and independent angular articulation each require a series of actuators and it may be desirable to reduce the number of actuators both for simplicity and quick controllability. In the configuration seen in Figure 61, the angular articulation of the second retractor member 1009 is surrendered with respect to the second frame section 1005, but the second frame section 1005 is made limitingly pivotable with respect to the first frame section 1003.

Beginning further discussion at the left of Figure 61, a threaded actuator 1111 includes a threaded shaft 1113, an expanded diameter actuator knob 1115, and a rotation capture fitting 1117 which will enable the threaded actuator 1111 to be captured axially and yet turn. The threaded actuator 1111 threaded shaft 1113 engages an internally threaded bore 1119 within the second frame section 1005 to enable it to be axially moved through the second retractor member 1009.

Second frame section 1005 includes a pair of internally disposed slots 1121, each of which is interrupted by a vertical accommodation slot 1123. Immediately adjacent the internally disposed slots 1121 are internally threaded bores 1125. The uppermost ends of the overall "U" shape of the second frame section 1005 includes an angled portion 1127 which is used in combination with other structures to limit the amount of pivot of the second frame section 1005 with respect to the first frame section 1003.

Second retractor member 1009 has thickened structurally reinforced upper head portion 1131 having a pair of outwardly disposed tongues 1133 which slidably fit within the slots 1121. Second retractor member 1009 has a lower extension member 1135 which may include an insertion accommodation slot 1137. The insertion accommodation slot 1137 has a lower extent which curves into the lower extension member 1135 to guide the terminal end of any member inserted into the insertion accommodation slot 1137 inwardly. Insertion accommodation slot 1137 has an upper end which opens from an upper surface of the reinforced upper head portion 1131.

A set screw 143 is seen over and insertable into a threaded bore 1145 which leads into a position to partially obstruct a bore (not seen in Figure 61) and capture the rotation capture fitting 1117 within the thickened structurally reinforced upper head portion 1131.

The first retractor member 1007 also has a thickened structurally reinforced upper head portion 1151, but has a pair of pivot bores 1153, one of which is visible in Figure 61. First retractor member 1007 also has a lower extension member

1155 which may also include an insertion accommodation slot 1157. The insertion accommodation slot 1157 has a lower extent which also curves into the lower extension member 1155 to guide the terminal end of any member inserted into the insertion accommodation slot 1157 inwardly. Insertion accommodation slot 1157 has an upper end which opens from an upper surface of the reinforced upper head portion 1151.

From an upper surface of the reinforced upper head portion 1151, an upper actuation block 1161 is seen as having a key slot 1163 extending vertically throughout its length. The vertical length of the key slot 1163 enables a member to both pull and push the upper actuation block 1161 as it angularly tilts since the key slot 1163 will operate to enable pushing and pulling throughout a range of angles assumed by the first retractor member 1007.

First frame section 1003 includes a more distal pair of frame pivot bores 1171, which are aligned with each other and also alignable with the internally threaded bores 1125 of second frame section 1005. First frame section 1003 also includes a less distal pair of internally threaded bores 1173, which are aligned with each other and also alignable with the pair of pivot bores 1153 of the reinforced upper head portion 1151 of the first retractor member 1007. A pair of internally threaded bores 1173 are engaged by a pair of externally threaded set screws 1175 to gather support to further engage pivot bores 1153 carried by the thickened structurally reinforced upper head portion 1151 of the first retractor member 1007. Threaded set screws 1175 enable first retractor member 1007 to pivot with respect to first frame section 1003.

Generally, the first frame section 1003 has a first level which includes the more distal pair of frame pivot bores 1171 and the less distal pair of internally threaded bores 1173. This level may be on a corresponding first level of second frame section 1005 and a same first level on second frame section 1005 is seen to include the internally threaded bores 1125, and the internally threaded bore 1119. As a result, the threaded actuator 1111 acts to move the second retractor member

1009 at a level directly across from the pivoting connection of the pivoting connection of the first retractor member 1007 to the first frame section 1003 and directly across from a pivoting connection of first frame section 1003 to second frame section 1005 (as will be shown).

A second level of first frame section 1003 is seen as a raised fitting 1181. The raised fitting 1181 is a block which supports an internally threaded bore 1183 at a second level, above the first level occupied by the more distal pair of frame pivot bores 1171 and the less distal pair of internally threaded bores 1173.

To the right of internally threaded bore 1183, a threaded actuator 1191 includes a threaded shaft 1193, an expanded diameter actuator knob 1195, and a rotation capture fitting 1197 which will enable the threaded actuator 1191 to be captured horizontally within the upper actuation block 1161 key slot 1163. Capture of the rotation capture fitting 1197 will allow it to urge the upper actuation block 1161 forward and rearward to cause the first retractor member 1007 to pivot. The key slot 1163 will continued engagement of the rotation capture fitting 1197 regardless of the angle of the first retractor member 1007.

A pair of main threaded members 1199 each have an externally threaded portion 1201 and a knob 1203. The threaded portions pass through the more distal pair of frame pivot bores 1171 and threadably engage the internally threaded bores 1125 of the second frame section 1005. The knobs 1203 of the pair of main threaded members 1199 can be tightened to fix the angle of the first frame section 1003 with respect to second frame section 1005. Also seen is a small bevel cut 1205 on the thickened structurally reinforced upper head portion 1151 to better enable the thickened structurally reinforced upper head portion 1151 to tilt forward.

Referring to Figure 62, a view of the assembled frame retractor system 1001 is seen. The co-planarity of the first and second frame sections 1003 and 1005 is seen. In the assembled position, it is more readily seen that the threaded

actuator 1191 can actuate the upper actuation block 1161 away from the raised fitting 1181. It can also be seen that the coplanarity of the first and second frame sections 1003 and 1005 can be maintained even as the thickened structurally reinforced upper head portion 1131 and lower extension member 1135 move parallel to the left.

Referring to Figure 63, a perspective view of the frame retractor system from the same perspective as seen in Figure 61 is illustrated as being fitted with a fiber optic illuminator seen as a length of fiber optic cable 1211 which is guided into the insertion accommodation slot 1137. As could be noted from Figures 61 and 62, the slot is a key-type slot having an opening into the inside of the lower extension member 1135. The fiber optic cable 1211 can thus be set to emit at a terminal end 1213, any point near the terminal end, or along the length of the lower extension member 1135 through the portion of the slot along the length of the lower extension member 1135.

Also noted in Figure 63 is the upward angular displacement of the second frame section 1005 with respect to the first frame section 1003. Note that the pivot axis is about a line between the knobs 1203, and through the more distal pair of frame pivot bores 1171 and pair of pivot bores 1153 which were better seen in Figure 61. Turn arrows are shown around the knobs 1203 as they can be slightly loosened or tightened to control the tension and capability to hold or change the angle of the second frame section 1005 with respect to the first frame section 1003.

Also note that regardless of the angular position of the second frame section 1005 with respect to the first frame section 1003 seen in Figures 61 and 62 that the threaded actuator 1111 can be independently manipulated to increase or decrease the distance the lower extension member 1135 occupies with respect to the lower extension member 1155. Independently of this, threaded actuator 1191 can be used to determine the angle which lower extension member 1155 takes with respect to first frame section 1003. The angular separation of the lower

extension member 1135 occupies with respect to the lower extension member 1155 seen in Figure 63 is due to the angular position of the second frame section 1005 with respect to the first frame section 1003. Further separation of the lower extension member 1135 occupies with respect to the lower extension member 1155 can be achieved by actuation of the expanded diameter actuator knob 1195.

Figure 64 is a top view of the frame retractor system 1001 seen in Figures 61-63. Also seen an anchoring structure 1221 held in by a threaded member 1223. The dashed line portions of the drawing of Figure 64 illustrate the action in moving the thickened structurally reinforced upper head portion 1131 and lower extension member 1135 along the second frame section 1005 by using the pair of outwardly disposed tongues 1133 within the pair of internally disposed slots 1121.

Referring to Figure 65, a bottom view of the frame retractor system 1001 seen in Figures 61-64 illustrates the nature of the insertion accommodation slots 1137 & 1157.

Referring to Figure 66 a plan view of the frame retractor system 1001 is seen. An additional structural connector 1227 is seen connected to the anchoring structure 1221.

Referring to Figure 67, a wire retractor 1251 is seen. Wire retractor 1251 has a scissors rear portion 1253 which is shown in a horizontal position and a generally vertical front portion 1255. As shown, the scissors rear portion may have a ratchet mechanism 1257 for helping to hold the scissors portion 1253 in a closed position which will hold generally vertical front portion 1255 in an open position.

Generally vertical front portion 1255 includes a pair of relatively thin members 1261 and 1263, which are connected to scissor arms 1265 and 1267, respectively. Thin member 1261, after an angular change 1271 from scissor arm 1265, includes a somewhat square inward detour as an accommodation portion 1273. Likewise, thin member 1263, after an angular change 1275 from scissor arm 1265, includes a somewhat square inward detour as an accommodation portion 1277.

Below and beyond the accommodation portions 1273 and 1277

each of the thin members 1261 and 1263 have a pair of wing extensions 1279. The wing extensions 1279 limit the ability of the relatively thin members 1261 and 1263 to move past one another, and limit the amount that the accommodation portions 1273 and 1277 actually do move past each other as will be seen.

Below the wing extensions 1279 the relatively thin members 1261 and 1263 each turn outward and taper to a point 1281. The point 1281 is used to penetrate muscle and to further stabilize the operational field. Referring to Figure 68, the relatively thin members 1261 and 1263 are shown in a position separated from each other, with the accommodation portions 1273 and 1277 being separated. The outwardly directed parts of the accommodation portions 1273 and 1277 are shown in a position to fit within the rounded upper opening of the frame retractor system 1001. This enables the practitioner to perform lateral retraction while "locking" the wire retractor 1251 into a stable position with respect to the frame retractor system 1001.

Referring to Figure 69, an isolated view of the generally vertical front portion 1255 illustrates the wire retractor shown superimposed in a crossing pattern to reduce the width profile for entry into the frame retractor system 1001 of Figures 61-66 even when the retractor system 1001 is in a position where the lower extension member 1135 is closest to lower extension member 1155.

Referring to Figure 70, a side view of the frame retractor system 1001 illustrates the position in which the wire retractor 1251 takes within the frame retractor system 1001. The lower extension member 1135 need only be slightly separated from the lower extension member 1155 to accommodate the wire retractor 1251. The wire retractor 1251 is simply used to hold back tissue which is already stressed below the bottom of the lower extension members 1135 and 1155 and need only transmit some retention forces to be effective.

Referring to Figure 71 illustrates the frame retractor system 1001 and wire retractor 1251 shown with respect to tissue 1285 and which is positioned over deeper tissues 1282.

Note that the pair of wing extensions 1279 are positioned close together. This is the position which the generally vertical front portion 1255 assumes upon insertion into the lower extension members 1135 & 1155 when lower extension members 1135 & 1155 are in close proximity to each other.

Referring to Figure 72, a view illustrating the wire retractor 1251 being opened to a stable open position within the frame retractor system 1001 is seen. The tissue 1285 to the sides are held back even where lower extension members 1135 & 1155 are separated from each other.

Referring to Figure 73, a manual tool 1283 includes a main handle portion 1284 supporting a forward fitting 1285. The fitting 1285 shown includes an internal bore and a key slot 1286. An interchangeable blade attachment 1287 has a rear end which includes a stop collar 1288 and a key projection 1289 which fits with respect to the key slot 1286. A working tip end of the interchangeable blade attachment 1287 includes a pair of oppositely disposed triangular blades 1288.

Referring to Figure 74, a different interchangeable blade attachment 1289 is shown as having a flat rounded end 1289. Referring to Figure 75, a manual tool 1290 is shown as having a slip fitting 1291 with manual register. A slip ring 1292 is movable toward the handle portion 1284 to unlock and away from the handle portion 1284 to lock. Figure 76 illustrates a view looking into the slip fitting 1292 and illustrates the concentric location of the slip ring 1292 surrounding a split ring portion 1293. A registry block 1294 is seen which insures that the interchangeable blade attachment 1449 cannot rotate on its axis when supported by the main handle portion 1443.

Referring to Figure 77, a top view of a further embodiment of a frame retractor system 1301 is shown. Referring to Figure 78, a bottom view of the embodiment of Figure 77 is shown. Referring to both Figures 77 and 78, a frame retractor system 1301 includes a first main frame member 1303 shown to the left and which has an overall outer dimension generally matching that of a second member section 1305. The tops and undersides of the first and second main frame members 1303 and 1305 have

formed depressions 1307 which are fitted with threaded bores (not shown) which fit with a series of threaded members 1309 and can be used to securely lock down any matching structure, with an inner contour of the depressions 1307 to match the outer contour of an object to be secured to first and second main frame members 1303 and 1305. One such object is shown as an anchoring structure 1311 having a curved portion matching an curved portion of the depression 1307.

The first main frame member 1303 surrounds a first inner pivotable frame member 1313. A pair of pivot pin members 1315 are shown as extending through bores 1317 at the opposite sides of the first main frame member 1303 and into blind pivot bores 1319 in the second frame section 1305. The pivot pin members 1315 may preferably have a threaded exterior engaging matching threads in bores 1319 to securely lock the pivot pin members 1315 in place.

The first main frame member 1303 is pivotally connected to the second main frame member 1305 by a similar pivoting arrangement. Pivot pins 1323 extend through bores 1325 in the first main frame member 1303, and into through bores 1327 in the second main frame member 1305. The pivot pins 1323 extend short of interference with an internal groove 1329.

The first inner pivotable frame member 1313 supports a first retractor half 1331 which includes a thickened structurally reinforced upper head portion 1333 and a lower extension member 1335. The upper head portion 1333 is sized to fit closely within the first inner pivotable frame member 1313 to facilitate quick change out. A pair of rotational locks 1337 secure the structurally reinforced upper head portion 1333 with respect to the first retractor half 1331. With this method and configuration, different sized retractors can be quickly selected and locked into the frame retractor system 1301 to enable retraction structures of different shape, depth, diameter and different accessory capability, to be used with the frame retractor system 1301. Rotational locks 1337 can be threaded members which lock the first retractor half 1331 by securing the top edge of the reinforced upper head portion 1333

down onto the inner pivotable frame member 1313. Rotational locks 1337 can also be cam members which rotate protrusions into slots carried by the reinforced upper head portion 1333.

The second frame member 1305 supports a first inner translatable frame member 1341 which is linearly translatable within the internal groove 1329 in the second frame member 1305. The first inner translatable frame member 1341 has a tongue 1343 which fits within the internal groove 1329 and has a length and other dimensions sufficient to stably support the first inner translatable frame member 1341 with respect to the second frame member 1305.

The first inner translatable frame member 1341 supports a second retractor half 1345 which includes a thickened structurally reinforced upper head portion 1347 and a lower extension member 1349. The upper head portion 1347 is also sized to fit closely within the first inner translatable frame member 1341, and is held in place by a pair of rotational locks 1337 in the same manner as upper head portion 1347. Both first and second retractor halves 1331 and 1345 can be quickly and easily changed. Also seen in the underside view of Figure 78 are bores 1351 in which the pair of rotational locks 1337 may operate.

There are three main mechanical controls seen in Figures 77 & 78. At the left side, a knob 1355 is attached to a threaded member 1357 which is threadably engaged into a raised block 1359 mounted atop first main frame member 1303. The threaded member 1357 continues beyond the threaded portion and terminates in a ball shaped fitting 1361. Ball shaped fitting 1361 is engaged in the axial direction by a rotational fitting block 1363. The rotational fitting block 1359 enables the threaded member 1357 to be urged axially forward and rearward by turning threaded engagement with the internally threaded raised block 1359 while urging the rotational fitting block 1363 toward and away from the raised block 1359 to cause the first inner pivotable frame member 1313 to pivot with respect to the first main frame member 1303.

At the right side a knob 1365 is attached to a threaded

member 1367 which is threadably engaged into a bore 1369 within second main frame member 1305. Threaded member 1367 continues beyond the threaded portion and terminates within first inner translatable frame member 1341. The threaded member 1367 has a groove 1371 for interfitting with a ring lock fitting 1373. The combination of the groove 1371 and ring lock fitting 1373 enables the threaded member 1367 to freely rotate within the first inner translatable frame member 1341 to cause the first inner translatable frame member 1341 to be moved along internal groove 1329.

As a result of the first two controls, the separation and angularity of the lower extension members 1335 and 1349 can be independently controlled. A third control controls the angularity of the first main frame member 1303 with respect to the second frame member 1305, and can somewhat equalize the angular position of the lower extension members 1335 and 1349 with respect to the average angle of the first and second main frame members 1303 and 1305.

Best seen in the lower portion of Figure 77, an adjustment knob 1375 is attached to a threaded member 1377. At the opposite end of threaded member 1377 a ball fitting structure 1379 is seen. The ball fitting structure 1379 rotatably fits within a rotational block fitting 1381 which may have a top opening to allow the threaded member 1377 to be rotated upward to disengage the rotational block fitting 1381.

The threaded portion of the threaded member 1377 fits inside a threaded support block 1383 having at least a portion of an internal space threaded (as shown in Figure 77). A detent mechanism may be supplied within the threaded support block 1383, including a threaded member 1385 capturing a spring 1387 which urges a detent ball 1389 into contact with the threads of threaded member 1377. Opposite the detent ball 1389 are at least a partial set of internal threads 1391 are seen. Where the internal threads 1391 are only lateral threads, the threaded member 1385 may be lifted up, out of contact with such internal threads 1391. This type of action is desirable where an obturator 33, 215 or 241 are or may be used to set the

angular displacement of the lower extension members 1335 and 1339.

In this case, and depending upon the detent setting, the surgeon can select between disengagement and remaining engagement of the mechanism, hereafter referred to as frame angle mechanism 1393 including adjustment knob 1375, threaded member 1377, ball fitting structure 1379, rotational block fitting 1381, threaded support block 1383, threaded member 1385, spring 1387 and a detent ball 1389, and internal threads 1391. The frame angle mechanism 1393, being located to the side of the working space, can be re-engaged at any time by turning the knob 1375 and threaded member 1377 to a position corresponding to the angular relationship of the first main frame member 1303 with respect to the second frame member 1305.

Also seen is an optional fiber optic system 1395 which can be utilized with the frame retractor system 1301 or any frame retractor system disclosed. The fiber optic system 1395 may be a laser source powered remotely, or it may simply be a support for a guided fiber optic. It is shown as being secured by the threaded members 1309 and has a terminus 1397 extends into the

Referring to Figure 79, a sectional view taken along line 79-79 of Figure 77 illustrates further details of the pair of pivot pin members 1315 and pivot pins 1323. Also seen more clearly is the internal groove 1329.

Referring to Figure 80, a sectional view taken along line 80-80 of Figure 77 illustrates further details of the inside of first inner translatable frame member 1341. The upper extent of the second retractor half 1345 is seen. A lower support surface 1401 is seen to provide an even resting place for thickened structurally reinforced upper head portion 1347. A rotatable member 1403 is seen as being rotatable between a locking position and an unlocked position.

Referring to Figure 81, a top semi sectional view sectional view focussing on the inside corner of the first inner translatable frame member 1341 illustrates further details of the locking mechanism. The upper extent of the second retractor half 1345 is seen. A rotatable member 1403

is seen as being rotatable between a locking position and an unlocked position. Rotatable member 1403 carries a flat side 1405 which can be rotated to face an indentation (to be shown) in either of the reinforced upper head portions 1333 or 1347 to allow such reinforced upper head portions 1333 or 1347 to slide out of held contact within the first inner pivotable frame member 1313 and the first inner translatable frame member 1341, respectively. Again, the configuration shown is but one of many physical realizations which will allow quick change-out and placement of the first and second retractor halves 1331 and 1345.

Referring to Figure 82 one of the indentations 1411 on the structurally reinforced upper head portion 1347 is seen. In the position shown, the rotational lock 1337 has been turned to present the flat side 1405 toward the structurally reinforced upper head portion 1347 and thus rotate the rounded side of the rotatable member 1403 out of occupation of the space of the indentation 1411 which allows upper head portion 1347 to be removed from the first inner translatable frame member 1341.

Further details of the first and second retractor halves 1331 and 1345 are shown in Figures 83 - 87. A broken line is seen in Figures 85 - 87 to illustrate variable length. Figure 83 is a bottom view of first retractor half 1331 looking up into the lower extension member 1335 and illustrating a cutout 1415 which can be considered a partial removal of material for enhanced ease of insertion and or registry with respect to an obturator, if desired.

Figure 84 is a bottom view of a second retractor half 1345 and also illustrating a complementary cutout 1415. Figure 85 is a side view the first retractor half 1331 shown in Figure 83 and illustrating a front profile of the cutout 1415. Figure 86 illustrates a matching side view the second retractor half 1345. Figure 87 is a view looking into the curved back side of second retractor half 1345 and illustrating a profile of the cutout 1415 illustrating it to be a an ark removing about half of the bottom periphery of the second retractor half 1345.

Further details of a second set of non-circularly curved

first and second retractor halves are seen in Figures 88 - 92. Again a broken line is seen in Figures 88 - 92 to illustrate variable length. The shape of Figures 88 - 92 provide a rectangularization of the viewing profile into the shape provided by the retractor halves to open the view space, yet retain the gentle curvature at the edges. Figure 88 is a bottom view of first retractor half first retractor half 1421 which includes a thickened structurally reinforced upper head portion 1423 and a lower extension member 1425. As before, the upper head portion 1423 is sized to fit closely within the first inner pivotable frame member 1313 to facilitate quick change out. As before indentations 1411 are present so that the structures shown in Figures 83 - 98 can be utilized with the frame retractor system 1301.

Figure 89 is a bottom view of a second retractor half 1427 and also illustrating complementary indentations 1411, upper head portion 1429 and lower extension member 1431. Figure 90 is a side view the first retractor half 1421 shown in Figure 88 and illustrating a side profile. Figure 91 illustrates a matching side view the second retractor half 1427. Figure 92 is a view looking into the rear back side and curving edges. Figures 93 and 94 illustrate a right side and rear view of a retractor half 1432 similar to that seen in Figures 88-92, but having a bulge 1433 at a middle but lower portion of the lower extension member 1425. Figures 95 and 96 illustrate a right side and rear view of a retractor half 1434 similar to that seen in Figures 88 - 92, but having a serrated shape 1435 formed along the bottom of the lower extension member 1425. Figures 97 and 98 illustrate a right side and rear view of a retractor half 1436 similar to that seen in Figures 88-92, but having a rounded cutout 1437 formed along the bottom of the lower extension member 1425.

Figure 99 illustrates a side elevation view taken somewhat with respect to the orientation seen in Figure 77 and looking into the side closest to the adjustment knob 1375. Details which are noticeable include the support of the threaded support block 1383 from the second frame member 1305. As can

be seen, the translation control of the first inner translatable frame member 1341 with the knob 1365 is had a lower or first level, generally at the levels of the first and second main frame members 1303 and 1305. The pivoting control of first inner pivotable frame member 1313 by the controlling engagement of the knob 1355 occurs a second level, above the levels of the first and second main frame members 1303 and 1305. It is also noted that the pivoting control of the first main frame member 1303 with respect to the second frame member 1305, via the control knob 1375, occurs at a level above the levels of the first and second main frame members 1303 and 1305.

In reality, translating control of the first inner translatable frame member 1341 with the knob 1365 can be accomplished with a fitting raised above the levels of the first and second main frame members 1303 and 1305. In addition, the pivoting control of first inner pivotable frame member 1313 with the knob 1355 can occur at the level of the first and second main frame members 1303 and 1305 by placing the support structures surrounding the pair of pivot pin members 1315 above or below the first and second main frame members 1303 and 1305. Similarly, the pivoting control of the first and second main frame members 1303 and 1305 with respect to each other can be had by placing the adjustment knob 1375, threaded member 1377 and ball fitting structure 1379 either at the level of the first and second main frame members 1303 and 1305 with placement of pivot moment structures elsewhere, or by placing the adjustment knob 1375, threaded member 1377 and ball fitting structure 1379 below the frame structure. Other mechanical structures for providing pivoting control of the first and second main frame members 1303 and 1305, each of the first inner pivotable frame member 1313 and first inner translatable frame member 1341 may be provided. Such other mechanical structures may provide for separate or integrated controls. Integrated controls may be provided electromechanically or mechanically and with or without the use of a microprocessor and pressure sensitive feedback sensing.

Continuing to refer to Figure 99, it can be seen that the surgical practitioner can adjust the positions of the lower extension members 1335 and 1339 in terms of their separation from each other regardless of angle, their angularity regardless of separation, and independently set the relationship of the first main frame member 1303 with respect to the second frame member 1305. Subsequent Figures 94 - 99 will illustrate only some of the movement possibilities.

Referring to Figure 100, a plan elevational view is shown similar to that seen in Figure 99, but with the frame retractor system 1301 shown from the opposite side from that seen in Figure 99. The knob 1365 has caused the threaded member 1367 to extend outside the second frame member 1305 to draw the first inner translatable frame member 1341 back into the second frame member 1305 to cause the lower extension member 1349 to move away from the lower extension member 1335.

Referring to Figure 101, a view from a common perspective as seen for Figure 100 illustrates the activation of knob 1375 has caused the threaded member 1377 to withdraw through the threaded support block 1383 to cause the first main frame member 1303 to move upwardly to form an angle with second frame member 1305. The ability to precisely control the angle of first main frame member 1303 with respect to the second frame member 1305 enables the user to adjust the mean or average position of the frame members 1303 and 1305 with respect to the general orientation of the extension members 1335 and 1349. This enables the user to avoid having the frame members 1303 and 1305 assume a mean angle with respect to each other which is not somewhat centered by the angle of the frame members 1303 with respect to frame member 1305.

Referring to Figures 102 and 103, a view from a common perspective as seen for Figures 96 and 97 illustrates the activation of knob 1355 has to cause the threaded member 1377 to either withdraw through the threaded support block 1359 to cause the first inner pivotable frame member 1313 to tilt the lower extension member 1335 toward the lower extension member 1349; or conversely to cause the threaded member 1377 to move

forward through the threaded support block 1359 to cause the first inner pivotable frame member 1313 to tilt the lower extension member 1335 away from the lower extension member 1349.

With regard to the description for Figure 101, it can readily be seen that an angular displacement of the lower extension member 1335 with respect to the lower extension member 1349 as seen in Figure 102 might be achieved by some angular displacement of the frame members 1303 with respect to frame member 1305, with the remainder of angular displacement being provided by actuation of the lower extension member 1335. Angular displacement of the frame members 1303 with respect to frame member 1305 can occur in either direction if a sufficient length of threaded member 1377 is provided.

Referring to Figures 104 and 105, a view from a common perspective as seen for Figures 100 - 103 illustrates the activation of knob 1365 has to cause the threaded member 1367 to either rotatably extend into the internally threaded second frame member 1305 to cause the first inner translatable frame member 1341 to move toward the first main frame member 1303 to move the lower extension member 1349 toward the lower extension member 1335 (as seen in Figure 104); or to rotatably withdraw from the internally threaded second frame member 1305 to cause the first inner translatable frame member 1341 to move away from the first main frame member 1303 to move the lower extension member 1349 away from lower extension member 1335 (as seen in Figure 99).

Referring to Figure 106, a top view having a position equivalent to the position seen in Figure 104 is shown. The first inner translatable frame member 1341 is in a position having been moved all the way toward the first inner pivotable frame member 1313 to have the lower extension members 1335 and 1349 into a circular profile forming a tube. Figure 106 illustrates that the structures which provide angular control of the first main frame member 1303 with respect to the second frame member 1305 are well clear of the tube formed by the lower extension members 1335 and 1349, and even clear of

adjacent structures, including thickened structurally reinforced upper head portions 1333 and 1347, as well as the first inner pivotable frame member 1313 and first inner translatable frame member 1341. Essentially, the angular control of the first main frame member 1303 with respect to the second frame member 1305 is restricted to a dimension which is about the width of the first and second main frame member 1303 and 1305.

Referring to Figure 107, the frame retractor system 1301 is shown with respect to the obturator 33 seen in Figure 1. The presence of the obturator 33 provides an additional conical spreading structure with the advance of the ends of the pair of spreading legs 39 and 41 just beyond the distal most portion of the lower extension members 1335 and 1349. As has been seen in Figure 14, the obturator 33 can provide force at a distance and can assist in separating the first and second main frame member 1303 and 1305.

Referring to Figure 108 an option for disengagement and re-engagement of the frame angle mechanism 1393 is seen. Where the threaded support block 1383 has an open upper portion such that the threaded member 1377 can be snapped out of the support block 1383 and pivoted upward, the detent ball 1389 can be removed from its rotational fitting block 1363 and removed. The obturator 33 can then be employed to manipulate the lower extension members 1335 and 1349. The threaded member 1377 can be replaced once the lower extension members 1335 and 1349 have been moved to the desired position. Once the threaded member 1377 is replaced, the obturator 33 can be removed. Again, where the spring 1387 and detent ball 1389 arrangement is permissibly loose, the obturator 33 can be operated against the frame angle mechanism 1393 as a force detent. In this mode, the obturator would force the extension members 1335 and 1349 as the frame angle mechanism 1393 clicks open to a desired position. In this arrangement, the obturator 33 does not operate on either of the first inner translatable frame member 1341 or first inner pivotable frame member 1313, both of which are expected to be non movable by the obturator 33, but

operates on the frame angle mechanism 1393.

Referring to Figure 109, a variation on the frame retractor system 1301 in Figures 77 - 102 is seen as a frame retractor system 1801. The portion of frame retractor system 1801 generally appearing in the right third of Figure 109 is the same as was shown in Figure 77, and these structures will retain their original numbering. Note that first and second main frame members 1803 and 1805 are slightly more compact and more closely fitting with respect to each other.

The frame retractor system 1301 relied upon force structure located in a spaced relationship from the pivot axis, externally located with respect to the frame retractor system 1301 to operate. The relied upon force structure for tilt typically involved a threaded member 1357 or 1377 which could be seen externally. In both of these cases the axis of the threaded member 1357 or 1377 were external to the main vertical extent of the main structural members of the frame retractor system 1301. The axis of the threaded members 1357 or 1377 can be displaced from the pivot axes they control and provide enhanced mechanical advantage.

The frame retractor system 1801 provides control generally within the vertical limits of a first and second main frame members 1803 and 1805. Mechanical advantage can be achieved by selection of the pitch of the gears which follow. The method of control is to provide a relatively low profile knob having a vertical shaft which contains a worm gear. The worm gear acts upon an gear having an effective horizontal axis to either tilt a structure equivalent to the prior first inner pivotable frame member 1313 or to tilt the a first main frame member 1803 with respect to the second main frame member 1805.

Referring to the lower left side of Figure 109, a first gear works cover 1811 is secured by a pair of threaded members 1813. A low profile knob 1815 extends upward from the level of the first gear works cover 1811 to provide for manual user control. A first inner pivotable frame member 1821 is similar to the first inner pivotable frame member 1313, but is shown as having some material removed to accommodate the mechanism being

described.

A pair of oppositely disposed pin members include a first pivot member 1825 and a second pivot member 1827. The first pivot member 1825 is set to have a terminal portion within first inner pivotable frame member 1821 which turns with the first inner pivotable frame member 1821. The second pivot member 1827 need only support the first inner pivotable frame member 1821 and allow it to pivot with respect to the second main frame members 1805.

The low profile knob 1815 is attached to a worm gear (not seen in Figure 109). Adjacent worm gear (not shown in Figure 109) an elongate cylindrical gear structure may be located which will rotate with first inner pivotable frame member 1821. Such a gear surface may be located on a special gear within the first inner pivotable frame member 1821, or in the alternative, such a gear surface may be formed on the external surface of the first inner pivotable frame member 1821. Since the first inner pivotable frame member 1821 need only tilt slightly, the arrangement for the pitch of the worm gear assembly can yield significant mechanical advantage. Further, because the angular displacement is small, the size of the gear elements (deeper wider grooves) should not be adversely impacted by a relatively high mechanical advantage.

A similar arrangement is had with respect to the angular adjustment of first main frame member 1803 with respect to second main frame member 1805. Referring to the bottom center of Figure 104, a second gear works cover 1841 is secured by a pair of threaded members 1843. A low profile knob 1845 extends upward from the level of the first gear works cover 1841 to provide for manual user control. The low profile knob 1845 and second gear works cover 1841 engages a portion of the second main frame member 1805 and moves the angular relationship of the first main frame member 1803 with respect to second frame member 1805.

A pair of oppositely disposed pin members include a first pivot member 1847 and a second pivot member 1849. The first pivot member 1847 is set to have a terminal portion within

first main frame member 1803 enables first main frame member 1803 to become angularly displaced from second main frame member 1805 while securing the pivot point between first main frame member 1803 and second main frame member 1805.

Again, the low profile knob 1845 is attached to a worm gear (not seen in Figure 109). Adjacent worm gear (not shown in Figure 109) may be an elongate cylindrical gear structure will be located which will rotate with first inner, pivotable frame member 1821. Such a gear surface may be located on a special gear within the first main frame member 1803, or in the alternative, such a gear surface may be formed on the external surface of the first main frame member 1803, such as the rounded area adjacent second main frame member 1805 near the pivot point.

As before, since the first and second main frame members 1803 and 1805 can change their relative angular position only slightly, the arrangement for the pitch of the worm gear assembly can yield significant mechanical advantage without sacrificing the size and depth of the gear elements.

Referring to Figure 110, a bottom view of the frame retractor system 1801 is shown and illustrating the underside elements. Referring to Figure 111, a side view illustrates further details of the frame retractor system 1801 seen in Figures 109 and 110. This pan semi sectional view illustrates a first worm gear 1851 associated with low profile knob 1815 and a second worm gear 1853 associated with low profile knob 1845. A first pivot gear 1861 is seen engaging the first worm gear 1851, while a second pivot gear 1863 is seen engaging the second worm gear 1853. The first and second pivot gears 1861 and 1863 may be completely circular or may be semi-circular. The showing of Figure 110 can be a partial showing or it can be a showing greater than what is provided as the angle of tilt will not be great.

One of the advantages seen in both the frame retractor systems 1301 and 1801 is the ability to remove the first and second retractor halves 1331 and 1345 vertically. This enables, without moving the overall frame retractor systems

1301 and 1801, the first and second retractor halves 1331 and 1345 to be removed or replaced. Removal and replacement can be achieved simply by actuation of the pair of rotational locks 1337. Such interchange ability can permit the surgical practitioner to quickly change out first and second retractor halves 1331 and 1345 for other types and depths of retractors, or to remove the retractors in favor of other structures.

Referring to Figure 112 the frame retractor system 1301 is shown with the first and second retractor halves 1331 and 1345 removed, and with the working sleeve 35, previously seen in Figure 1, suspended with a clamp fixture 1901. As can be seen, clamped fixture 1901 has a base portion 1903 which is attached onto one of the formed depressions 1307 and secured by the series of threaded members 1309 which remain readily available for quick attachment of any utility structure. Referring to Figure 113, the base 1903 can be seen as extending across to a horizontal web portion 1906, and then upward to a strap portion 1907. The end of the strap portion is attached to the a nut 201 and bolt 203 assembly previously seen in Figure 25. Other strap supports can be employed on both the frame retractor systems 1301 and 1801 to enable wide flexibility in use.

In all of the devices shown, including the retractors devices such as working sleeves 35, 222; retractors 555, 571, 691, 573, 631, 657, 691, 751, 901, 1001, 1301, 1801 and obturators 33, 241, a manual control was shown including knobs 50, 587, 597, 597, 617, 627, 635, 673, 797, 1115, 1195, 1355, 1365, 1375, 1815, 1845 and more, as well as threaded member 203, and knob 261. Some are shown as knurled members and others as hexagonal members, but in fact the hexagonal shapes and knurled shapes can be used interchangeably.

Depending upon the size of the tool, its working depth and other factors, tremendous working forces can be generated. A review of the literature illustrates resort to massive mechanical members which project far from the medical instrument are often employed to generate the forces needed. The approach to all of the medical instrumentation herein has been one of low profile, and to occupy no more of the surgical

field than is absolutely necessary. Where the actuation members lie parallel and close to the patient's body they may be more difficult to actuate in the presence of significant tissue resistance to retraction. Therefore, a sterilizable ratchet has been developed in order to enable quick, temporary, enhanced mechanical actuation of the retractor members. Mechanical advantage may thus be had based upon mechanical advantage embodied in the particular retractor operation structure (including obturators) and in addition by a sterilizable ratchet tool which gives *even more precise* control for the medical practitioner. Any ratchet engagement is possible. A hexagonal bore could be provided within the knurled knobs to facilitate both direct manual and ratchet driven operation.

Referring to Figure 114 a ratchet actuation tool 3001 is shown. One of the problems with tools used in surgery is the ability to dis-assemble and sterilize and dis-assemble, if necessary the instrumentation. A ratchet or other common mechanical tool which would otherwise be a great help in the surgical theater is a problem from a sterilization standpoint. Most commonly known mechanisms include closed spaces, snap fit, and are not intended for disassembly. The ratchet actuation tool 3001 utilizes one-way permitted turning with a pair of socket heads and utilizes a simplistic internal mechanism with flow-through liquid wetting.

Figure 114 is a side view looking through the ratchet actuation tool 3001. The ratchet actuation tool 3001 includes a first socket 3003 having a socket opening 3005 shown in dashed format. A first plate 3009 includes an aperture (not shown in Figure 114) which provides rotational support. A second plate 3011 is spaced apart from the first plate 3009. An "open air" or through opening to the other side is labeled as 3013. To the left of through opening 3013 is seen a spring 3021, and spring bias post 3025 which is seen extending into the first plate 3009. A threaded member 3027 is seen attaching the end of the spring to a ratchet sprocket engagement head 3029. The ratchet sprocket engagement head 3029 engages a

sprocket 3031.

All of the components located just above the lower plate 3009, have a liquid gap between those components and either the first plate 3009 and second plate 3011, meaning that the components are not tightly jammed together to have a danger of creating significant sealed spaces. A second socket 3035 has a socket opening 3037. Second socket 3035 extends above second plate 3011. The first socket 3003 includes a through member having a threaded post which a matching threaded bore within the second socket 3035 which engages the threaded post. In the case of a right hand thread, the turning of the plates 3009 and 3011 and post will cause the second socket to be even more securely turned and locked onto the post. The use of a double socket design enables reliance upon turning in only one direction.

At the opposite end of the ratchet actuation tool 3001, a spacer clip 3045 has a spacer portion 3051 and a threaded bore 3053. A hook portion 3055 includes a rising vertical portion and a hook to help hold the second plate toward the first plate. A threaded member 3059 holds the spacer clip 3045 down into an accommodation space 3061.

The spacer portion 3051 has a height in excess of the depth of the accommodation space 3061 which will positively and securely set the height of the first plate 3009 with respect to the second plate 3011. The threaded member passes through a bore 3065 before it engages the threaded bore 3053. A groove 3067 is seen to extend partially around a cutaway 3069 with the groove to accommodate the forward portion of the hook portion 3055 and the cutaway 3069 to accommodate the bulk of the hook 3055. As can be seen, the removal of the threaded member 3059 causes spacer clip 3053 to fall away and frees the first plate 3009 from the second plate 3011 at the end opposite the first and second sockets 3003 and 3035.

Also shown is a round pivot bar 3071 which is preferably jam fit within a bore 3075 in the first plate 3009 and extends through the ratchet sprocket engagement head 3029 and then loosely through a bore 3077 in the second plate 3011.

Referring to Figure 115, a view is shown with the second plate 3011 removed, but with the spacer clip 3045 having been re-attached to show its position. Additional elements seen include the round pivot bar 3071 and the forward end 3081 of the ratchet sprocket engagement head 3029. The spring 3021 can be seen as acting on the ratchet sprocket engagement head 3029 to urge the forward end 3081 of the ratchet sprocket engagement head 3029 into locking contact with the sprocket 3031.

The sprocket 3031 is seen as having a square opening 3091. A threaded post 3093 has threads on the round portion shown and has a lower square member for interfitting with the square opening 3091 of the sprocket 3031. Referring to Figure 118, a view with many of the elements seen in Figure 115 is shown. The jam fit round pivot bar 3071 remains after the assembly consisting of the spring 3021, threaded member 3027, and ratchet sprocket engagement head 3029 is removed. Removal of the first socket 3003 reveals a first large aperture 3095 through which the threaded post 3093 extended in the assembled state.

Referring to Figure 117, a view of the top plate 3009 illustrates a second large aperture 3097. Also seen are the previously mentioned bore 3077, groove 3067 and cutaway 3069. Referring to Figure 118, a side sectional view of the first plate 3009 also illustrates a jam aperture 3099 previously occupied by the spring bias post 3025. Referring to Figure 119, a side sectional view of the second plate 3011 illustrates another view of the second large aperture 3097.

Other figures illustrate further details. Referring to Figure 120 an end view looking into the first socket 3003 is shown. Referring to Figure 121, a plan view of the first socket 3003 illustrate the details thereof. A stepped surface 3103 is larger than the first large aperture 3095 and prevents the first socket 3003 from passing through the first large aperture 3095. A rectangular section 3107 engages square opening 3091 of the sprocket 3031. This enables engagement of the ratchet sprocket engagement head 3029 onto the sprocket 3031 to translate into rotational fixation of the first socket

3003. Above the rectangular section 3107 is a threaded section 3109 which will engage a matching threaded bore in the second socket 3035.

Referring to Figure 123 a rear view of the second socket 3035 reveals a threaded bore 3111. Note that the ratchet sprocket engagement head 3029 is set to turn the threaded section 3109 clockwise into the threaded bore 3111. If the first and second plates 3009 and 3011 move in an opposite direction the sprocket 3031 moves in the other direction and simply causes the ratchet sprocket engagement head 3029 to click past the sprocket teeth. Figures 124 and 125 illustrate further details of the second socket 3035.

Referring to Figures 126 and 127 a plan and end view of the ratchet sprocket engagement head 3029 is seen in an unengaged position and without threaded member 3027. Newly seen is a main ratchet sprocket engagement head aperture 3121. Also seen is the threaded bore 3125 which is normally engaged by threaded member 3027 to hold spring 3021 in place.

Referring to Figure 128, a plan view of the sprocket 3031 is seen. Referring to Figure 129, a plan view looking downward on the spacer clip 3045 illustrates further details of the spacer clip 3045, and especially the relationship of the threaded bore 3053 to the forward hook portion 3055.

Figure 130 is an exploded sectional detail illustrating the relationship of the first plate 3009 and second plate 3011, how the spacer clip 3045 is secured to the first plate 3009, how the spacer clip 3045 secures the second plate 3011 and how the spacer clip 3045 acts to control the spacing between the first and second plates 3009 and 3011.

The retractor systems thus described permit the following surgical procedure, some steps of which may be omitted and the order of which is not necessarily in accord with the order of steps as presented:

1. Paraspinal incision at the level of a facet joint determined by fluoroscopy.
2. Insertion of Guide Pin to determine depth from skin to facet joint.

3. Apply the proper length surgical retractor blades to the frame.
4. Make an appropriate length incision, which may include:
 - (a) one and a half times the largest diameter for microdiscectomy procedure
 - (b) two times the width for two level fusion
 - (c) three times the width for three level fusion
5. Insert not more than one fascial incisor/tissue dissector over the Guide Pin and incise the fascia.
6. Dissect the muscle attachments of the multifidus muscles off the spinous process, lamina, and transverse process in a longitudinal direction.
7. Insert retractor with fitted obturator into the wound and verify correct placement with fluoroscopy.
8. Partially expand the obturator and retractor blades then remove the obturator.
9. Adjust the frame to the contour of the body with proper flexion or extension of the frame.
10. Connect the frame to the operating table or other support if desired.
11. Expand the retractor blades sufficient to visualize the planned surgical procedure.
12. Dock the tip of the retractor blades to the correct anatomical site.
13. Apply the custom Gelpi-type hand held retractor to retract muscle ingress if necessary.
14. Proceed with planned surgery.
15. Make changes of the position as necessary during the surgery and relax the retractor blades every twenty minutes to allow recirculation for of the muscles and nerves.

The advantages of performing a surgical procedure with the retractor systems described in the specification, include, but are not limited to the following:

1. A single entry process can be practiced instead of

- sequential two dilation process.
2. Creation of a surgical field is done only to the necessary dimension with micro adjustable frame and retractor blades.
 3. The use of an expanding obturator allows controlled separation of the muscle fibers so as to eliminate shredding and tearing of muscle.
 4. Customized retractor tips to allow docking on specific bony sites to further stabilize exposure.
 5. Surgical blade rotation is finely controllable with a threaded screw device giving both control and mechanical advantage.
 6. The retractor support is adjustable to body contour.
 7. Muscle compression release can be more easily carried out more often, such as every twenty minutes, for example.
 8. The retraction system is stable enough, that once deployed, such that attachment to the operating table may or may not be required.

While the present system has been described in terms of a system of instruments and procedures for facilitating the performance of a microscopic lumbar diskectomy procedure, one skilled in the art will realize that the structure and techniques of the present system can be applied to many appliances including any appliance which utilizes the embodiments of the instrumentation of the system or any process which utilizes the steps of the inventive system.

Although the system of the invention has been derived with reference to particular illustrative embodiments thereof, many changes and modifications of the systems shown may become apparent to those skilled in the art without departing from the spirit and scope of the inventive system. Therefore, included within the patent warranted hereon are all such changes and modifications as may reasonably and properly be included within the scope of this contribution to the art.

WHAT IS CLAIMED:

1. A minimal incision maximal access minimal invasive surgical spine instrument comprising:
 - a first retractor member(421, 753, 1007, 1331, 1421);
 - a second retractor member(423, 757, 1009, 1345, 1427);
 - a support (573, 631, 657, 691, 751, 901, 1001, 1301, 1801)having a first member (801, 945, 1003, 1303, 1803) for supporting said first retractor member and a second member (803, 947, 1005, 1305, 1805) for supporting said second retractor member, said first member (801, 945, 1003, 1303, 1803) of said support controllably angularly pivotable with respect to said second member (801, 945, 1003, 1303, 1803) of said support, and wherein at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427)is movable independent of its associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805).
2. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said a first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) have a pivot axis and wherein said having a first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) have a mechanical linkage for manipulating said first member (801, 945, 1003, 1303, 1803) with respect to said second member (803, 947, 1005, 1305, 1805).
3. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 2 wherein said mechanical linkage further comprises a hinge box (811) and wherein said first member (801, 945, 1003, 1303, 1803) has a first series of gear teeth (863) and wherein said second member (803, 947, 1005, 1305, 1805) has a second series of gear teeth (863) which intermesh with said first series of gear teeth

(863) to control the pivot of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) with respect to said hinge box (811).

4. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 2 wherein said mechanical linkage further comprises a first tilt adjustment fitting (951) associated with said first member (801, 945, 1003, 1303, 1803) and a second tilt adjustment fitting (953) associated with said second member (803, 947, 1005, 1305, 1805), said tilt adjustment fittings (951, 953) also associated with at least one main support (921, 923), to enable said first member (801, 945, 1003, 1303, 1803) to be controllably pivoted with respect to said second member (803, 947, 1005, 1305, 1805).

5. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 2 wherein said mechanical linkage further comprises a threaded support block (1383) supported by at least one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805), a threaded member (1377) having a ball fitting structure (1379) and having threads engaging said threaded support block (1383), and a rotational block fitting (1381) engaging the other of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) to enable said first member (801, 945, 1003, 1303, 1803) to be controllably pivoted with respect to said second member (803, 947, 1005, 1305, 1805).

6. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 2 wherein said mechanical linkage further comprises a first worm gear (1853) supported by at least one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805), and a pivot gear structure (1863) engaging the other of said first member (801, 945, 1003, 1303, 1803) and said second

member (803, 947, 1005, 1305, 1805) to enable said first member (801, 945, 1003, 1303, 1803) to be controllably pivoted with respect to said second member (803, 947, 1005, 1305, 1805).

7. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427)is movable independent of its associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) is a translating movement.

8. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427) has translating movement by the movement of at least one portion of said first member (801, 945, 1003, 1303, 1803) toward and away from said second member (803, 947, 1005, 1305, 1805).

9. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427) has translating movement by the movement of least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427) within its associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805).

10. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein at least one of said a first and second retractor members,(421, 753, 1007, 1331, 1421)(423, 757, 1009, 1345, 1427)includes a projection (577, 579, 601, 603, 1133, 1343) and wherein its

associated one of said first and second members (801, 945, 1003, 1303, 1803), (803, 947, 1005, 1305, 1805) includes a slot (575, 1121, 1329) in which said projection (577, 579, 601, 603, 1133, 1343) is guided to facilitate said translating movement.

11. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427)is movable independent of its associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) is a pivoting movement.

12. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427)has pivoting movement by a mechanical linkage for manipulating said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427) with respect to its associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) and wherein said mechanical linkage further comprises a threaded support block (847, 1181) supported by said associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805), a threaded member (795, 1193) having a ball fitting structure (791, 1161) and having threads engaging said threaded support block (847, 1181), and a rotational block fitting (793, 1161) engaging said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009, 1345, 1427).

13. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member(421, 753, 1007, 1331, 1421) and said second retractor member(423, 757, 1009,

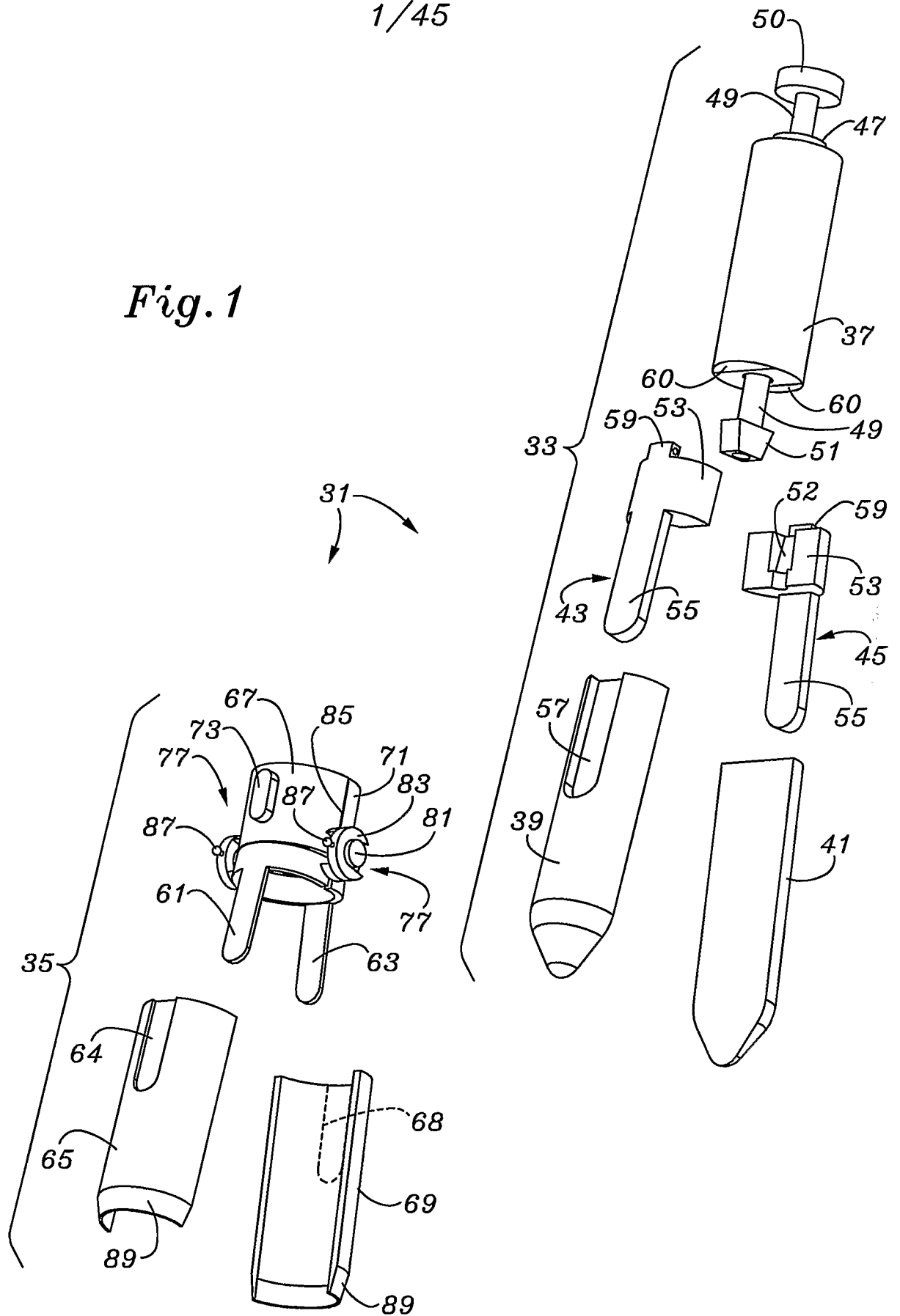
1345, 1427) has pivoting movement by a mechanical linkage for manipulating said at least one of said a first retractor member (421, 753, 1007, 1331, 1421) and said second retractor member (423, 757, 1009, 1345, 1427) with respect to its associated one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805) and wherein said mechanical linkage further comprises a first worm gear (1851) supported by at least one of said first member (801, 945, 1003, 1303, 1803) and said second member (803, 947, 1005, 1305, 1805), and a pivot gear structure (1861) engaging said at least one of said a first retractor member (421, 753, 1007, 1331, 1421) and said second retractor member (423, 757, 1009, 1345, 1427).

14. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 1 wherein said at least one of said a first retractor member (421, 753, 1007, 1331, 1421) and said second retractor member (423, 757, 1009, 1345, 1427) further comprises a frame member (1313, 1341) and wherein said frame member (1313, 1341) supports said at least one of said a first retractor member (421, 753, 1007, 1331, 1421) and said second retractor member (423, 757, 1009, 1345, 1427).

15. The minimal incision maximal access minimal invasive surgical spine instrument as recited in claim 14 wherein said at least one of said a first retractor member (421, 753, 1007, 1331, 1421) and said second retractor member (423, 757, 1009, 1345, 1427) is held within said frame member (1313, 1341) by rotational locks (1337) which engage said frame member (1313, 1341) by at least one of directly and laterally.

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Fig. 1



2/45

Fig. 2

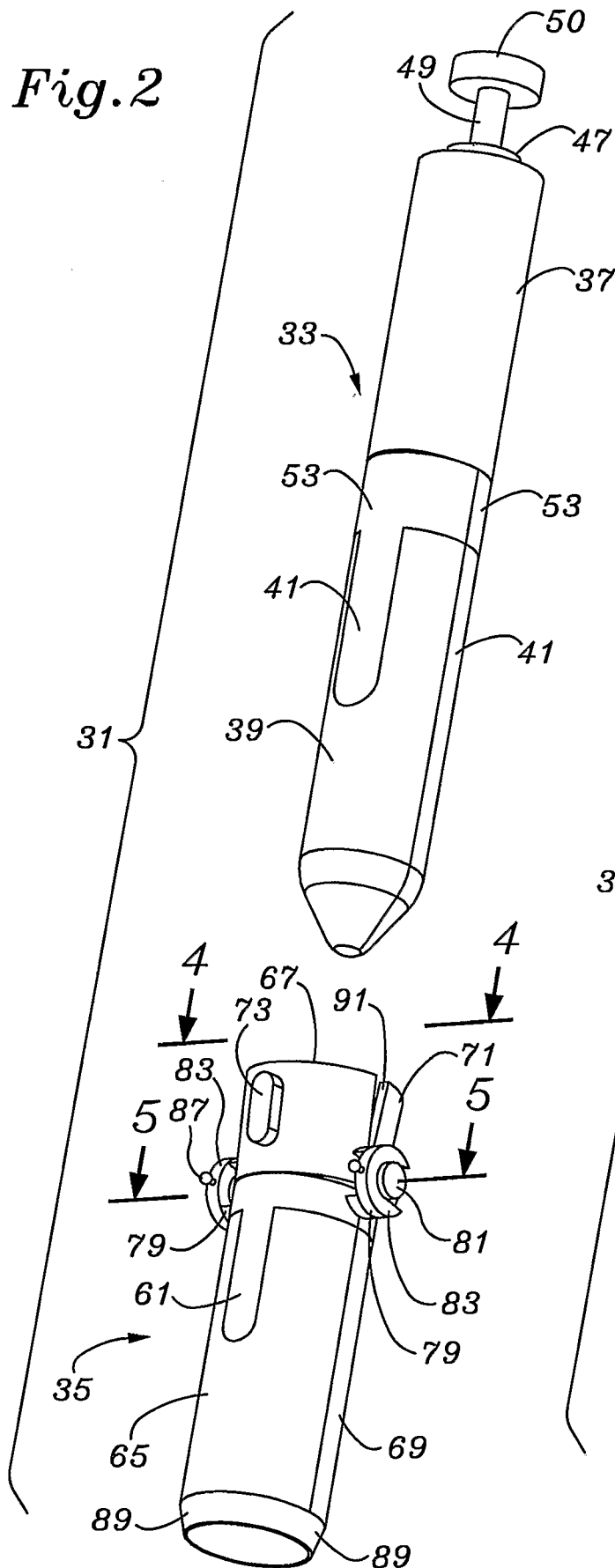


Fig. 3

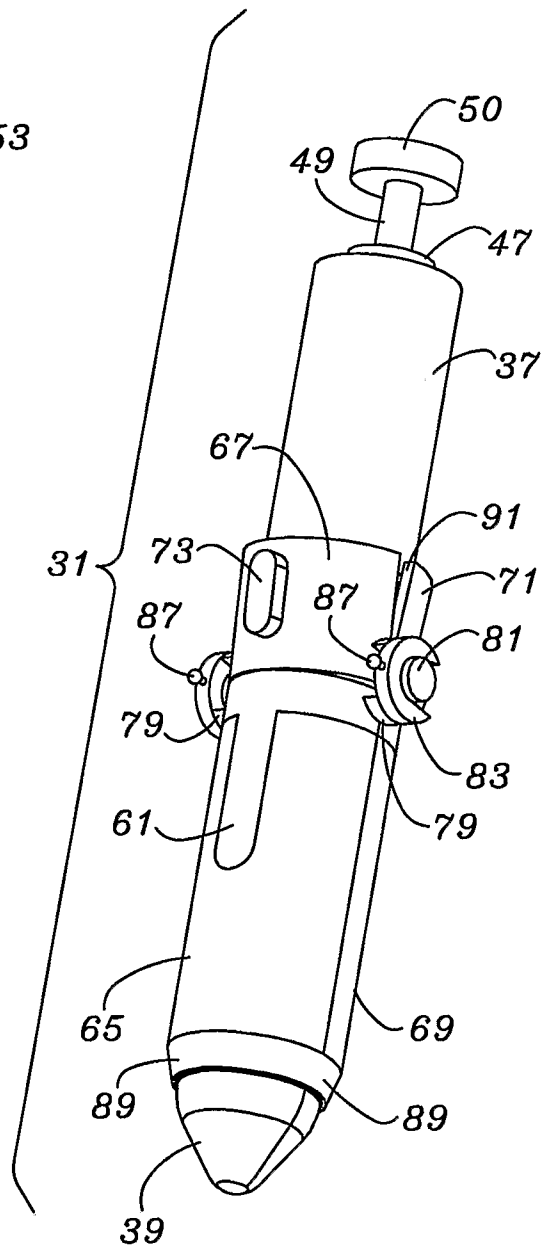


Fig. 4

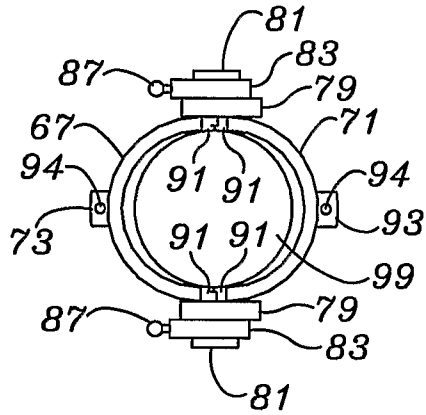


Fig. 5

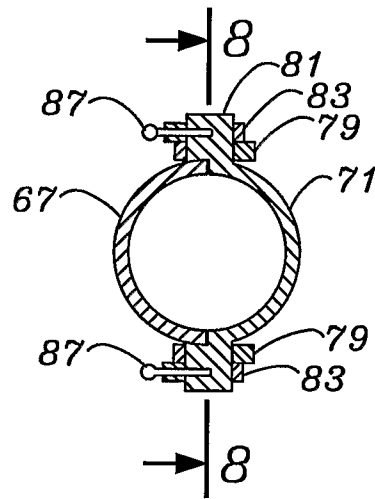


Fig. 6

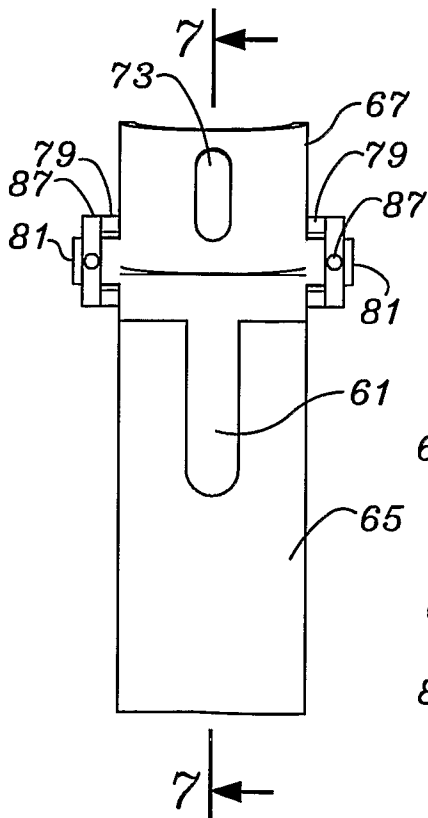


Fig. 7

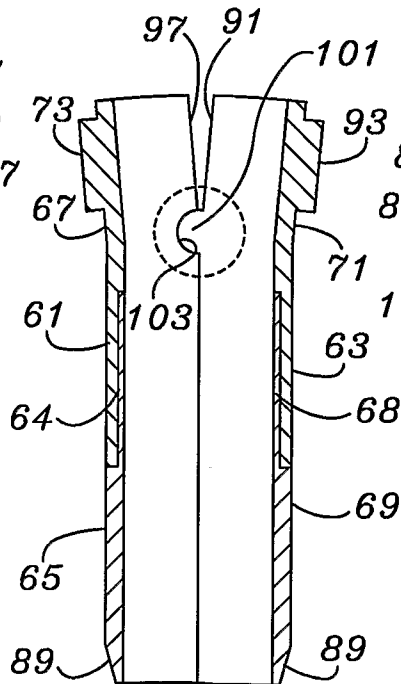
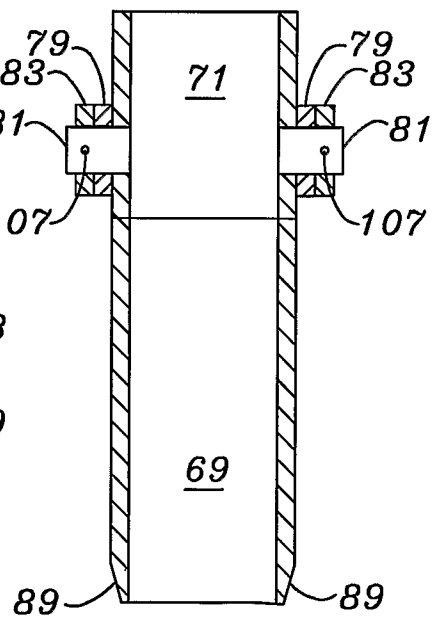


Fig. 8



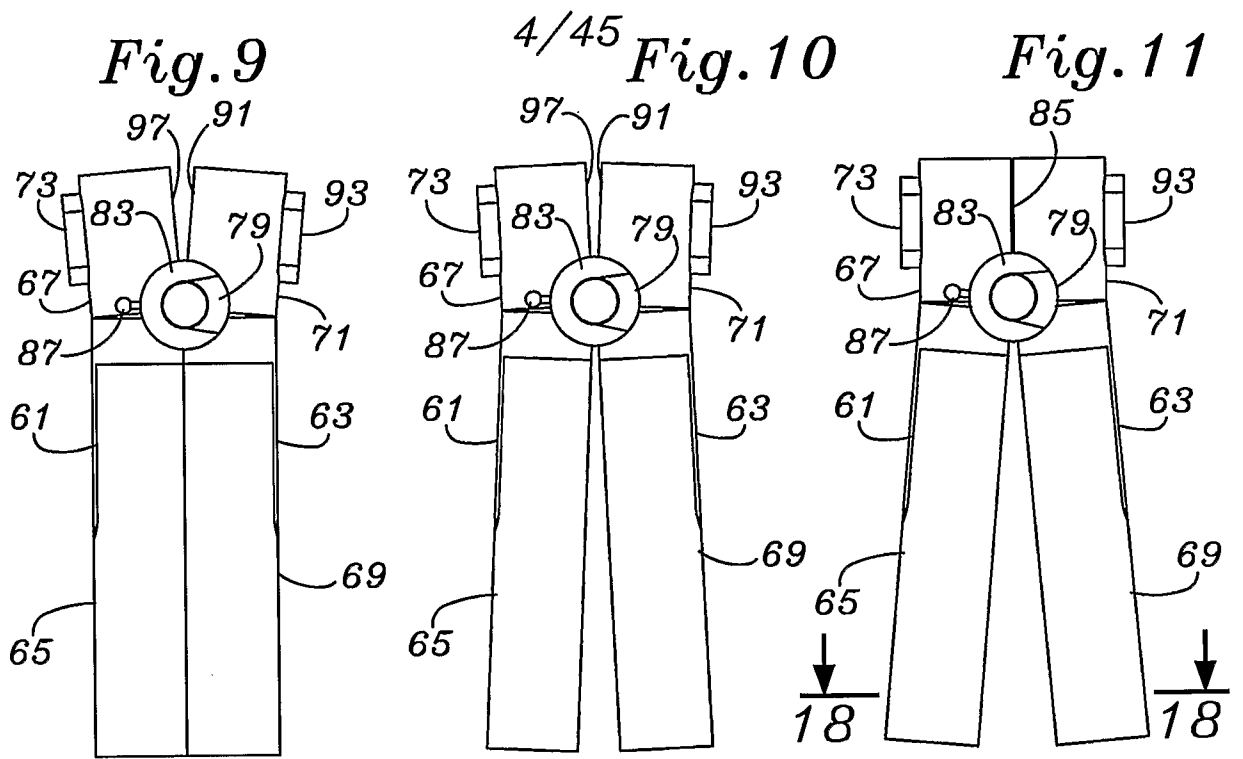


Fig. 12

Fig. 13

Fig. 14

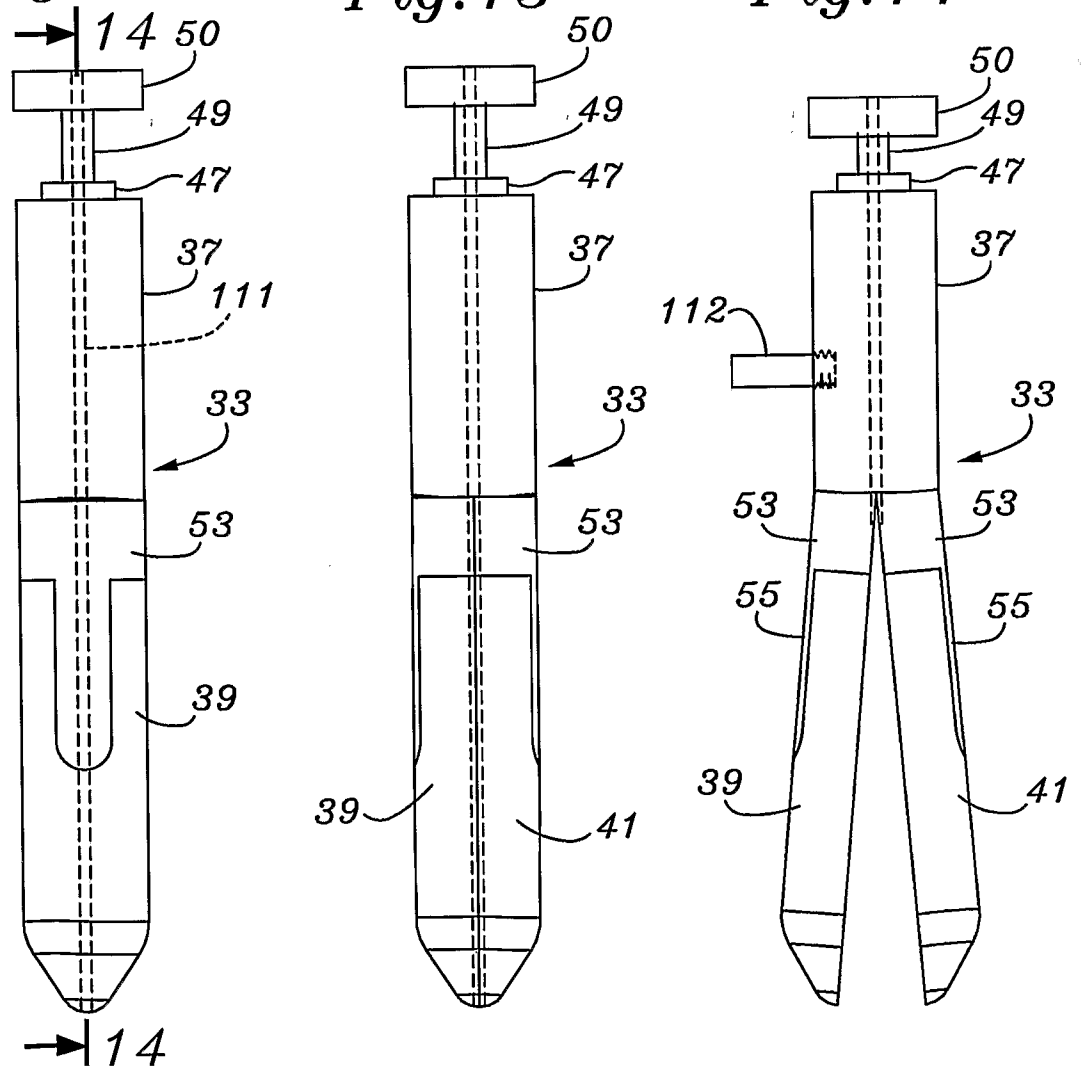


Fig. 17

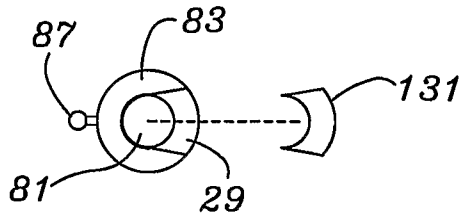


Fig. 18

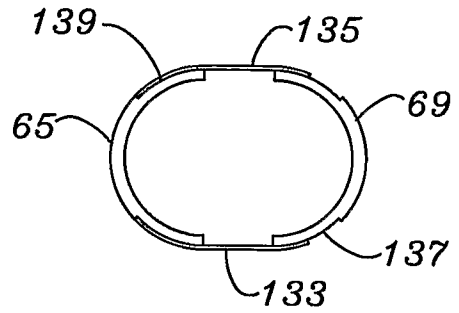


Fig. 15

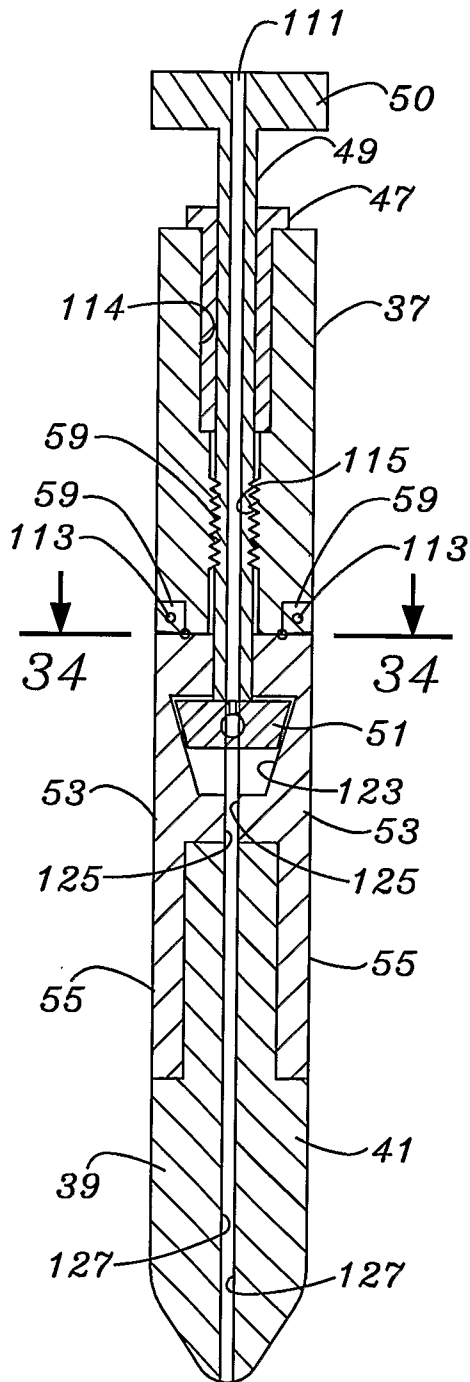
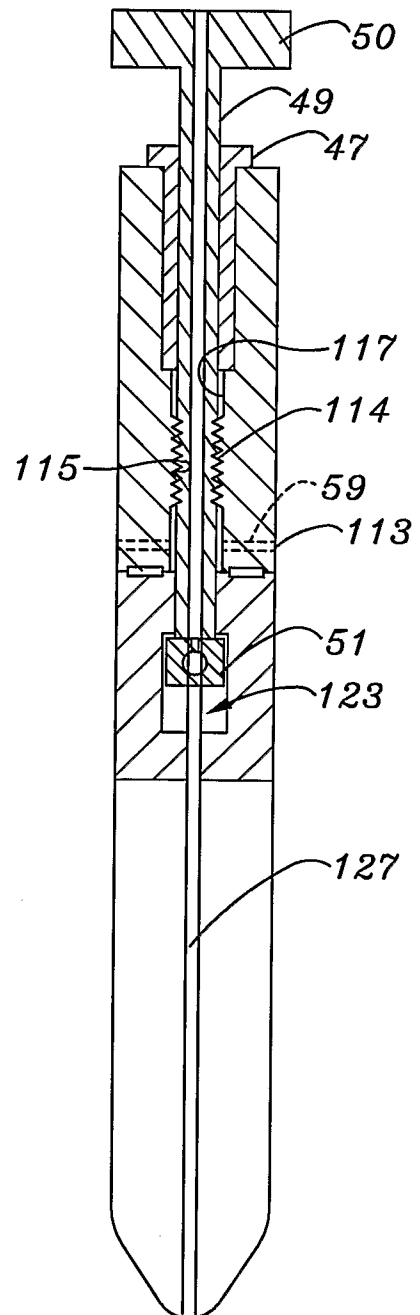


Fig. 16



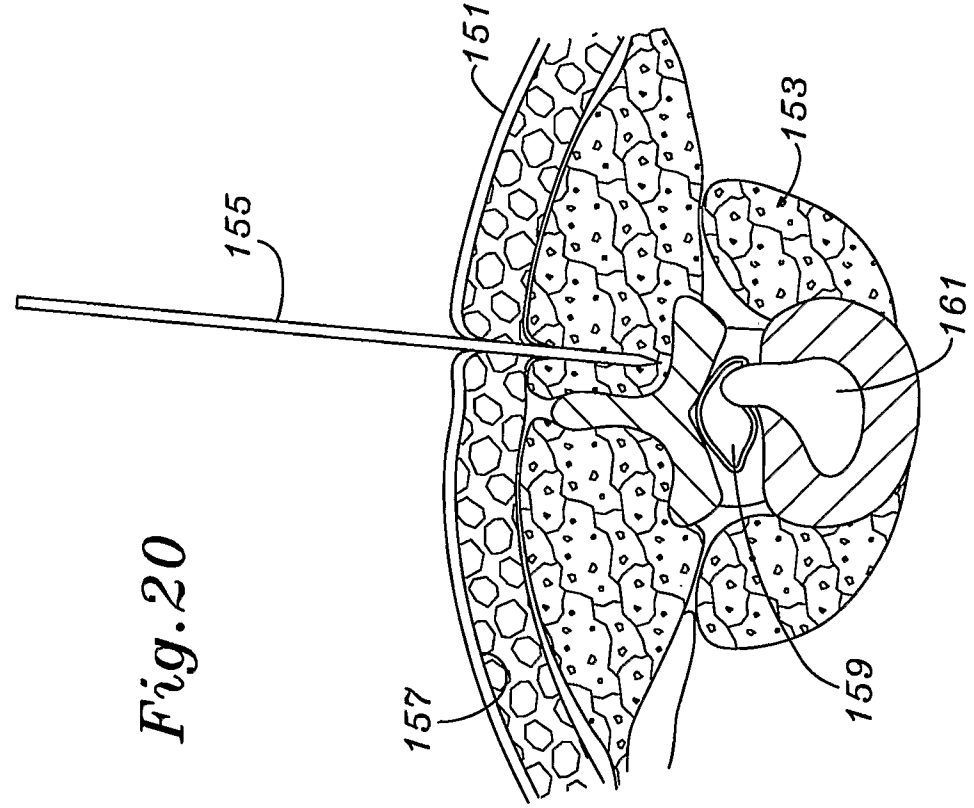


Fig. 20

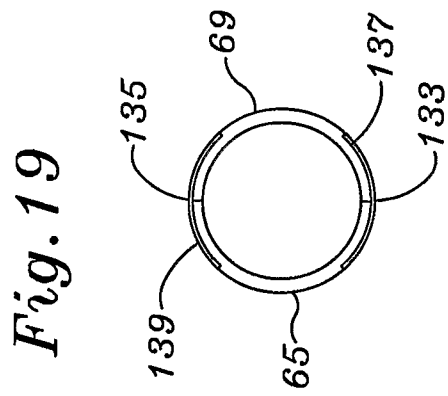


Fig. 19

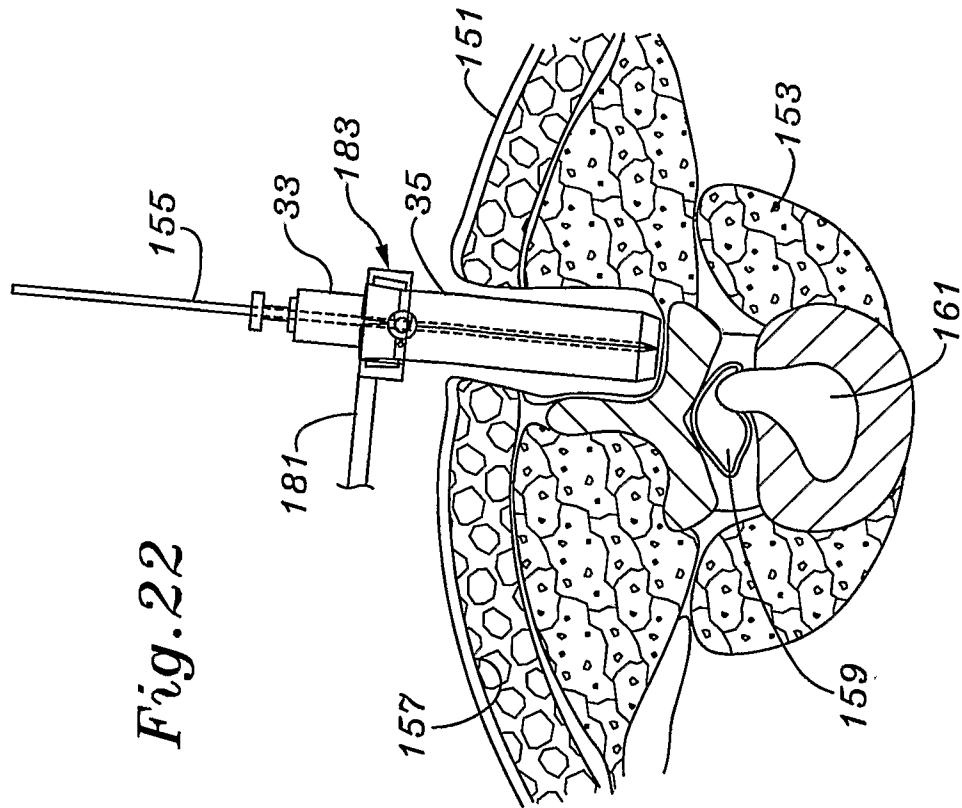


Fig. 22

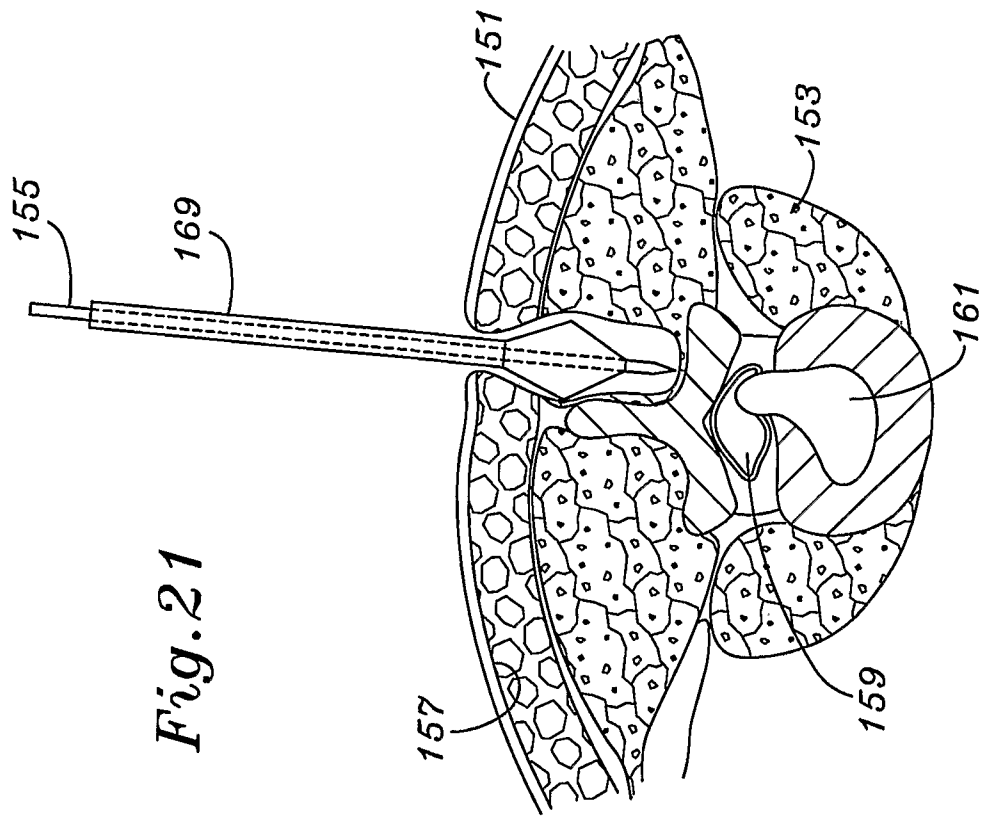


Fig. 21

Fig. 24

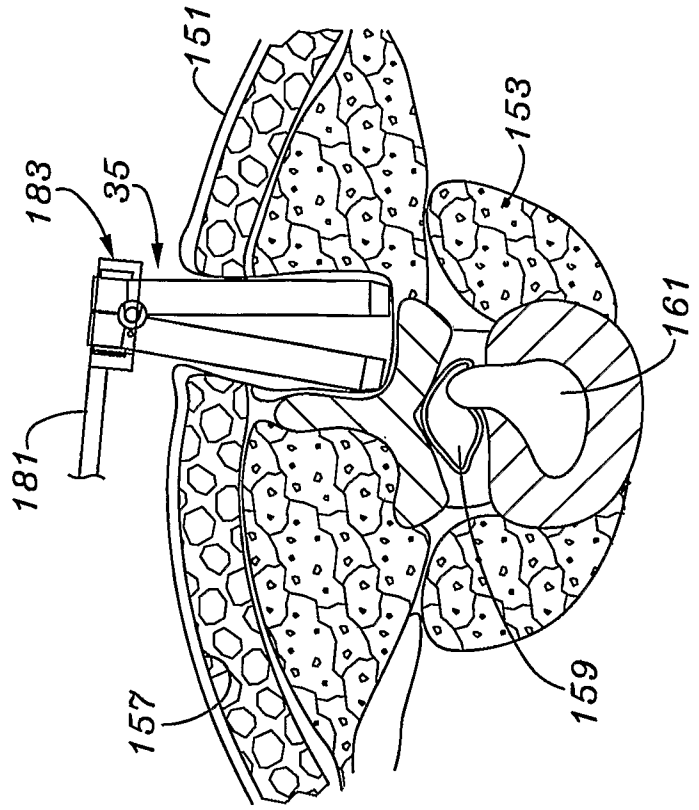


Fig. 23

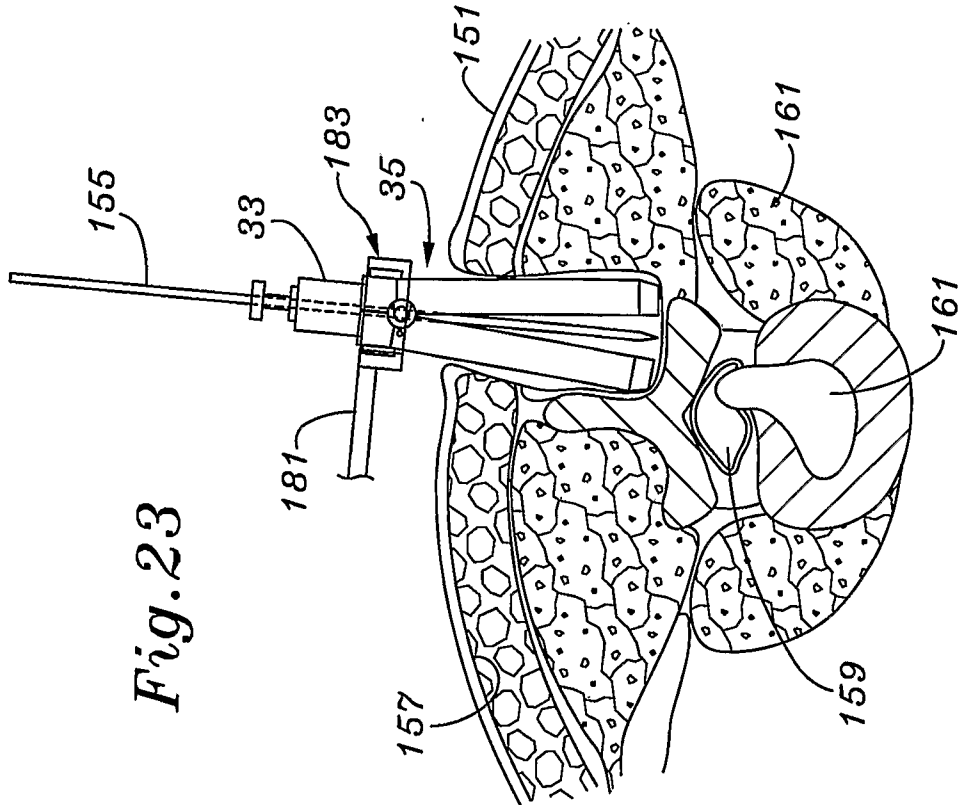


Fig. 25

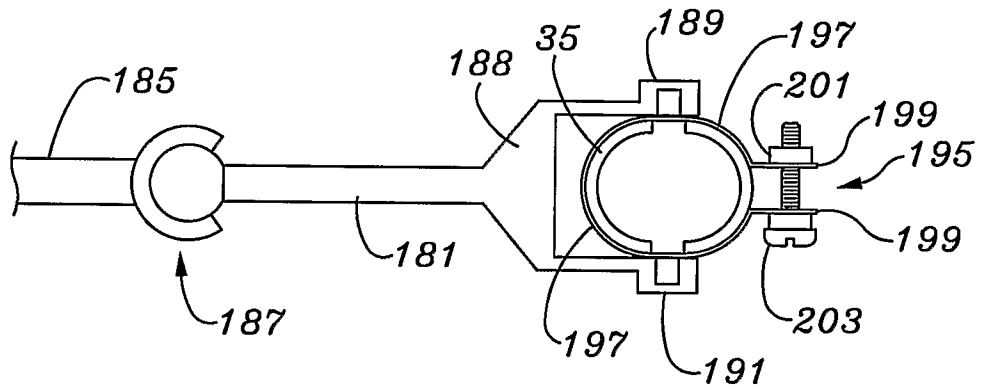


Fig. 26

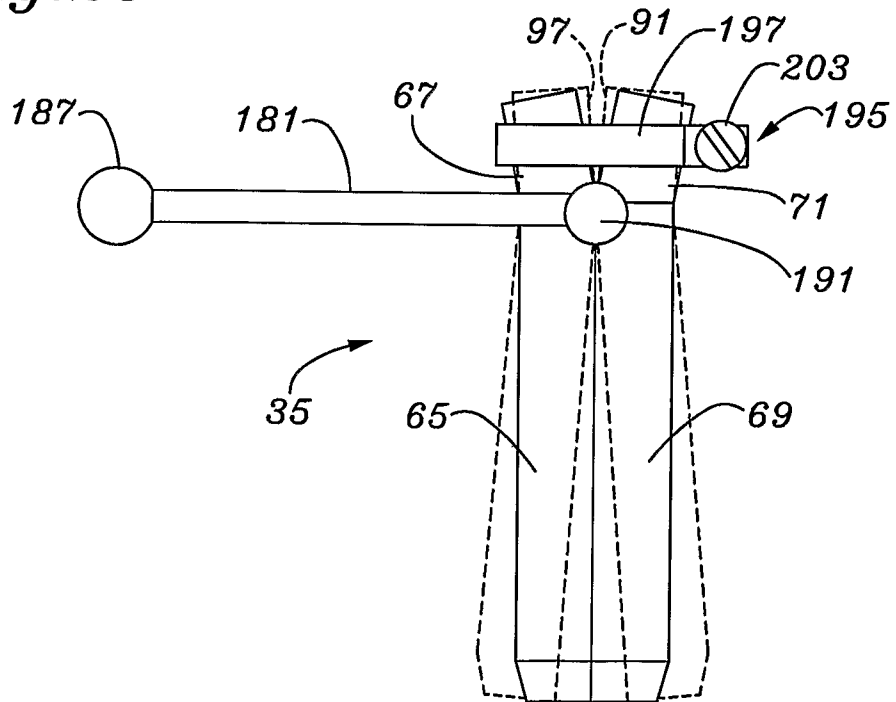


Fig.27

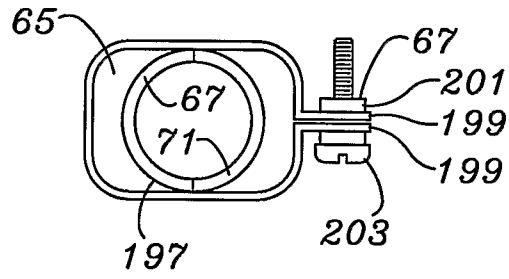


Fig.28

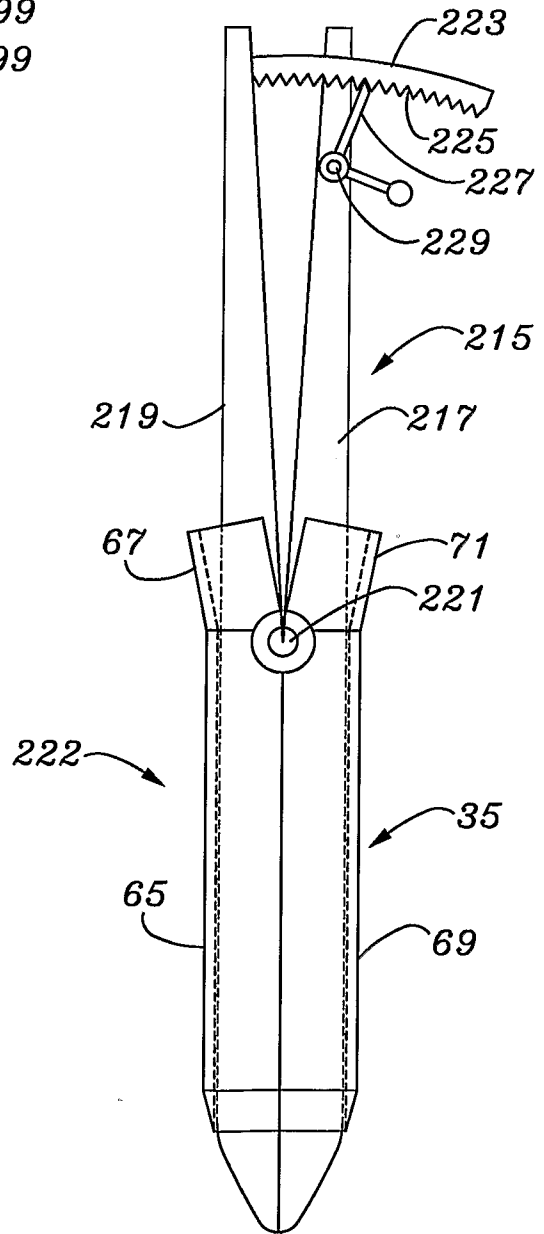


Fig. 29 11/45

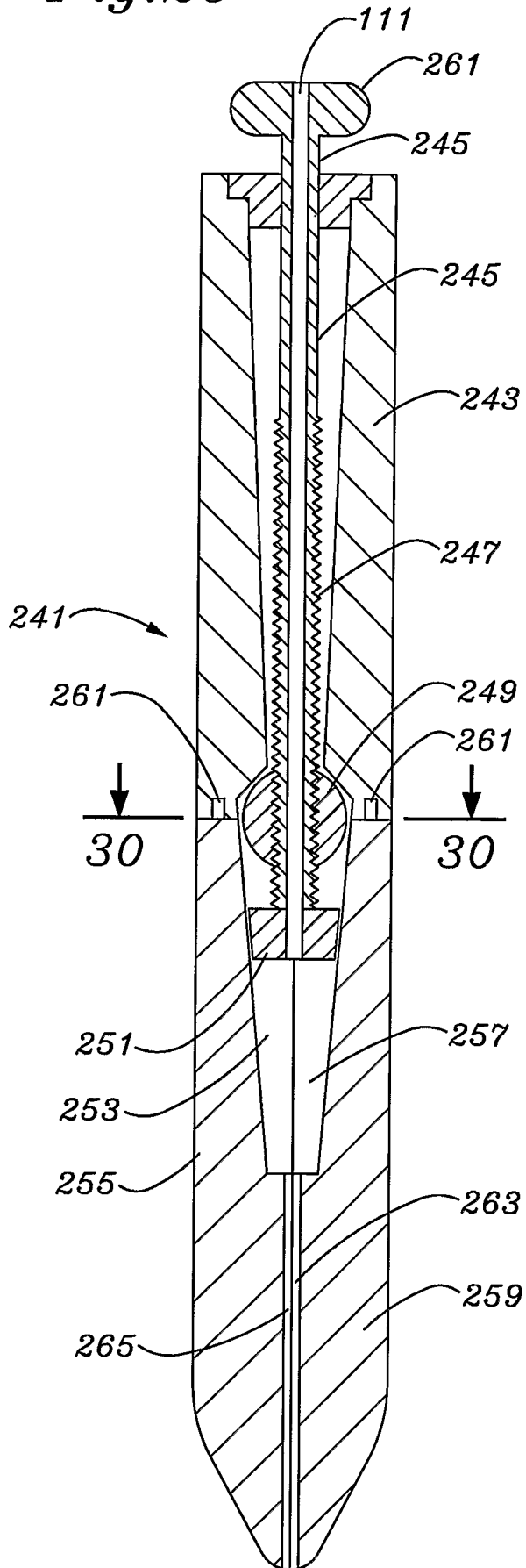


Fig. 31

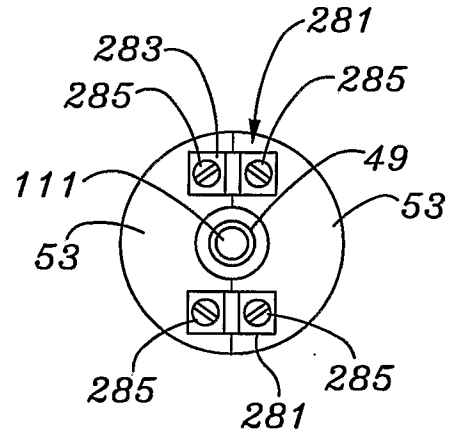


Fig. 30

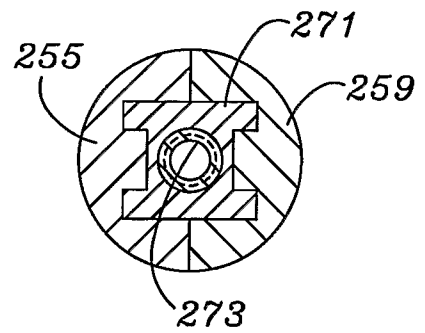


Fig. 32

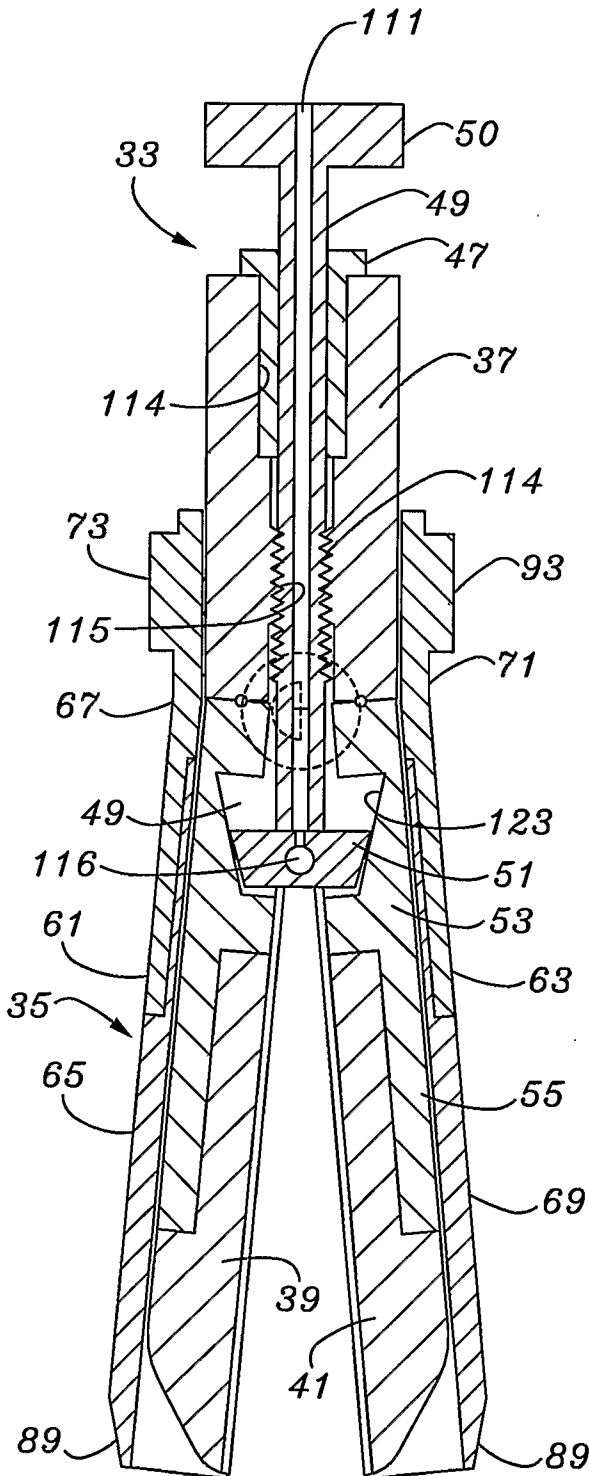


Fig. 33

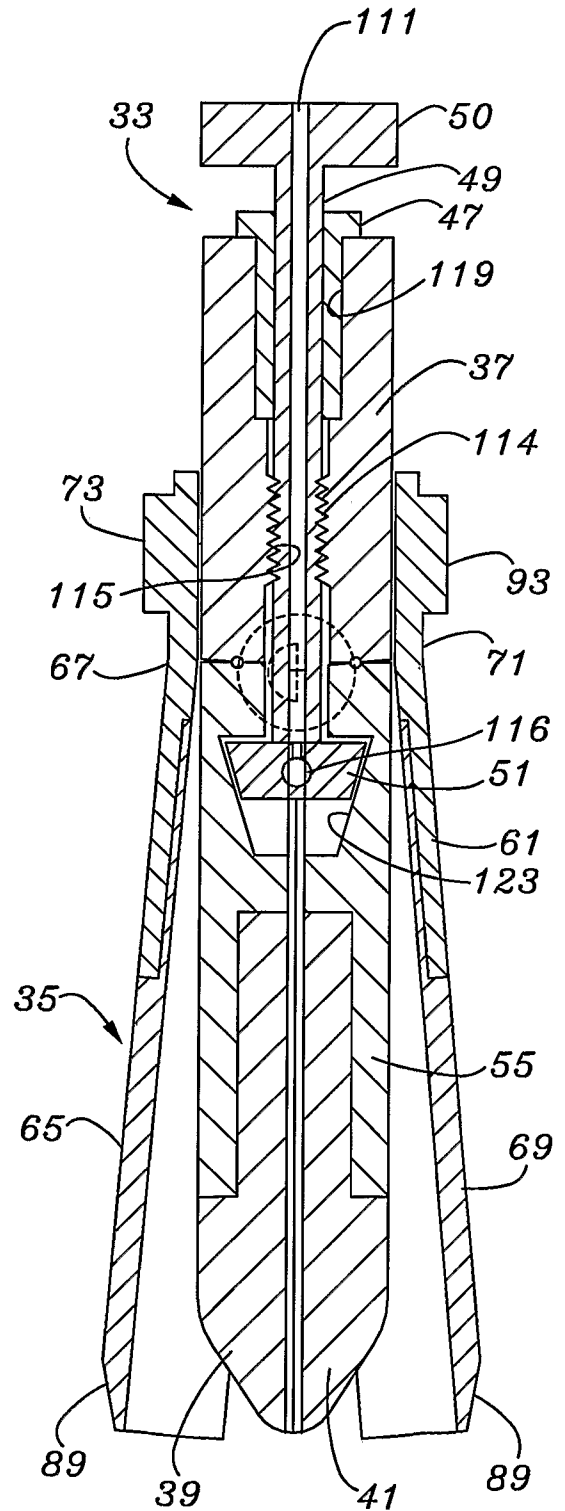


Fig. 34

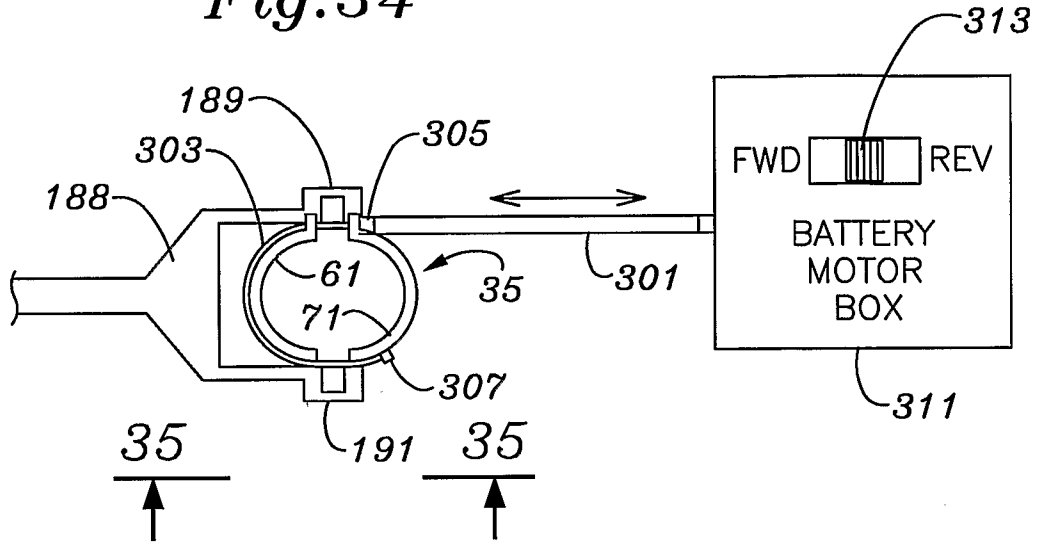


Fig. 35

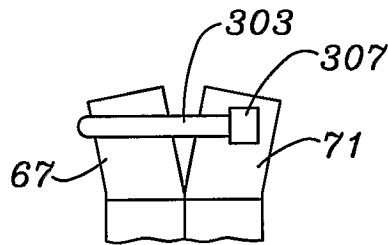


Fig. 36

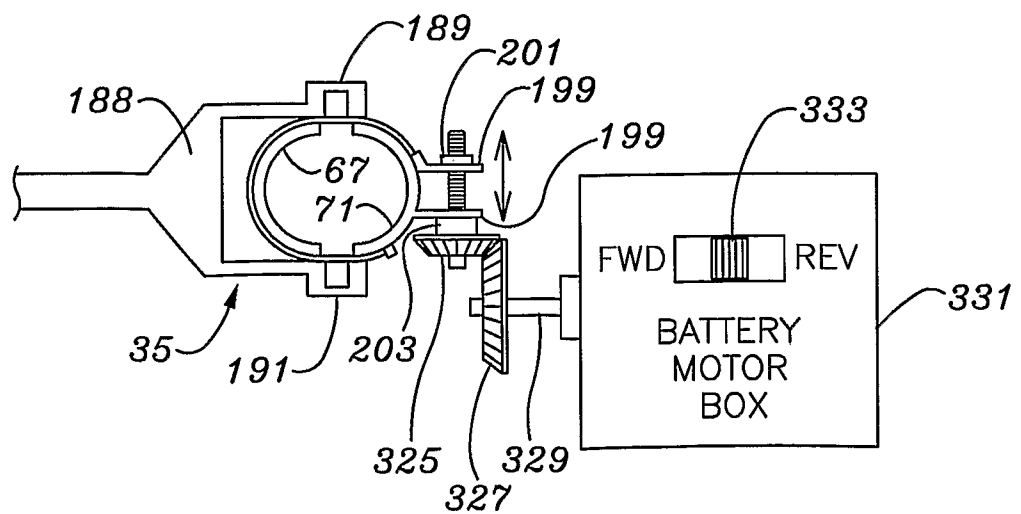


Fig.37

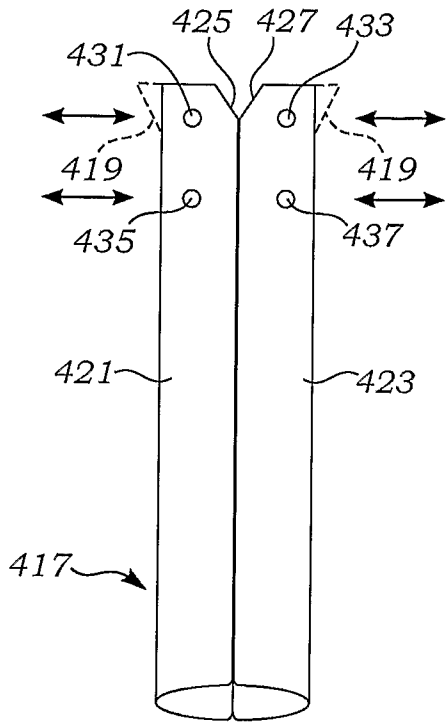


Fig.38

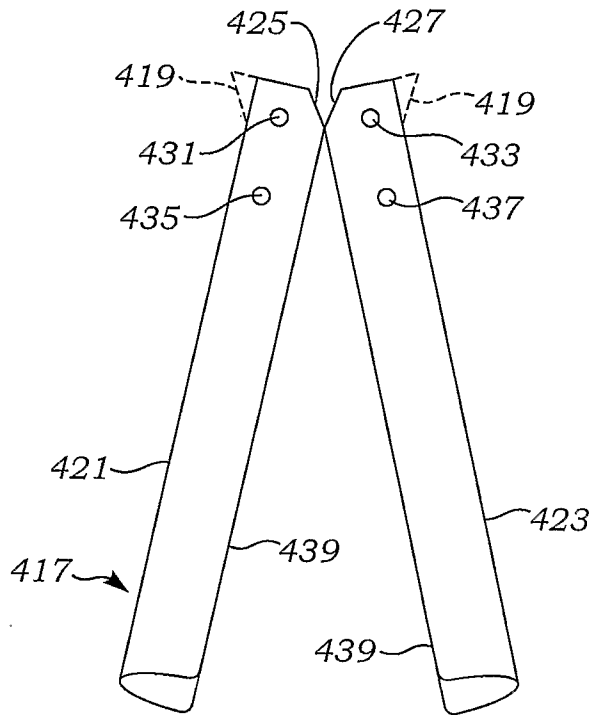


Fig.39

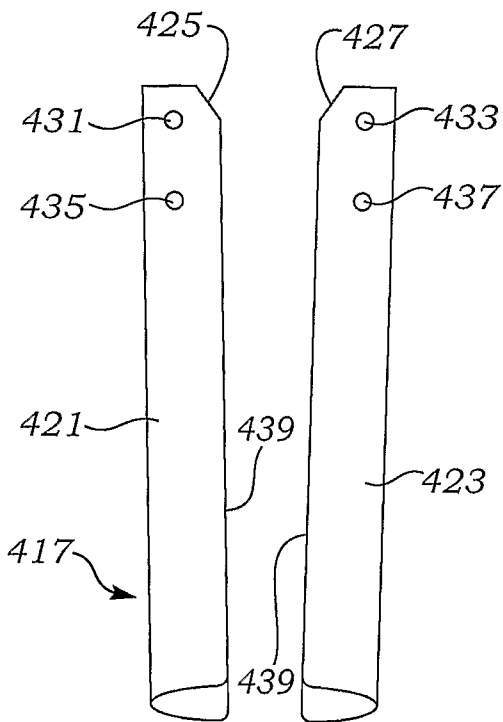


Fig.40

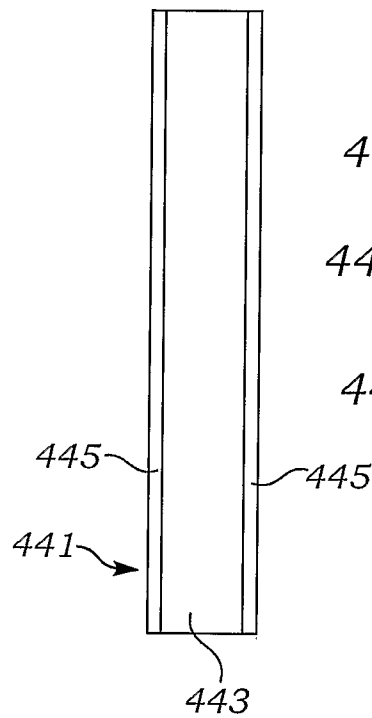


Fig.41

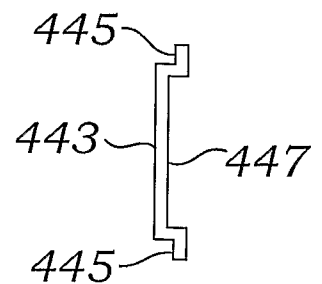


Fig.42

Fig.43

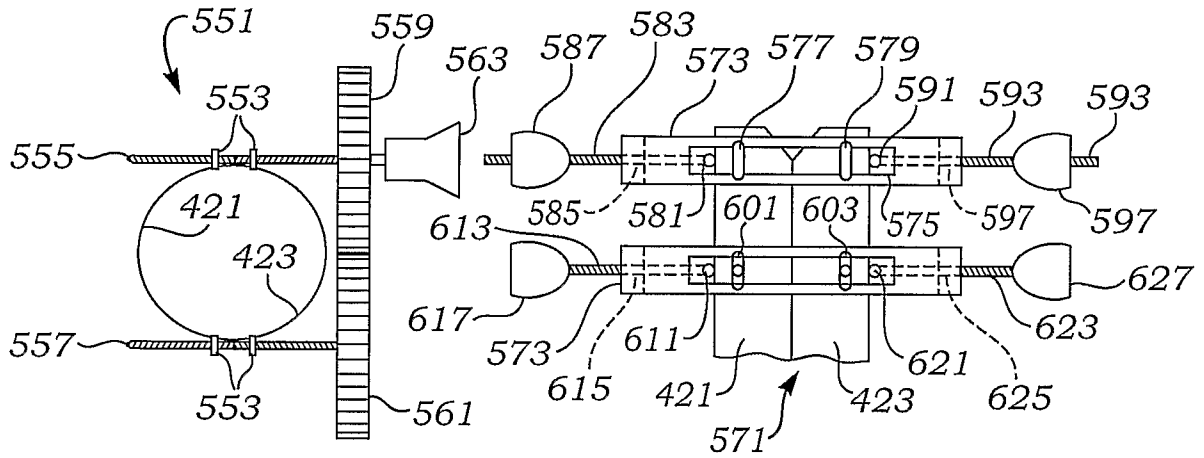


Fig.44

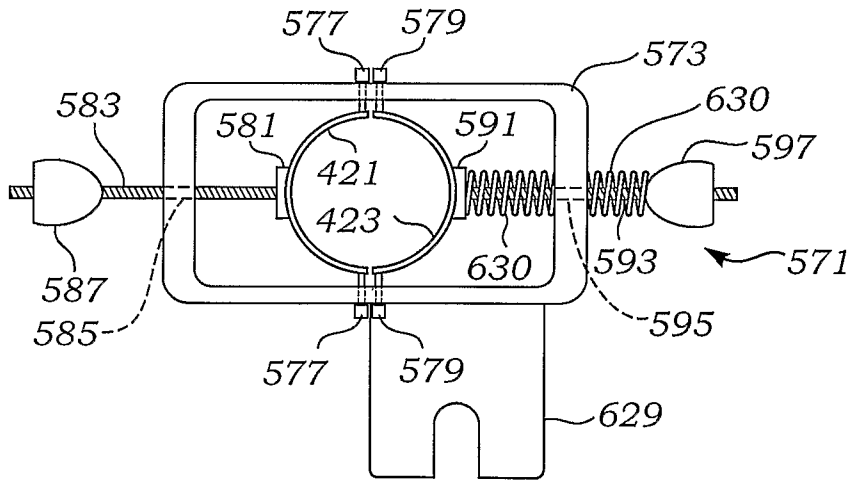
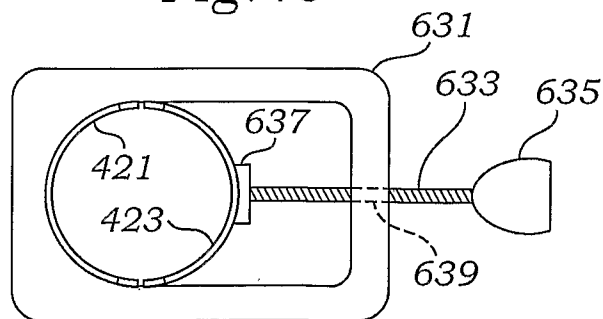


Fig.45



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Fig.46

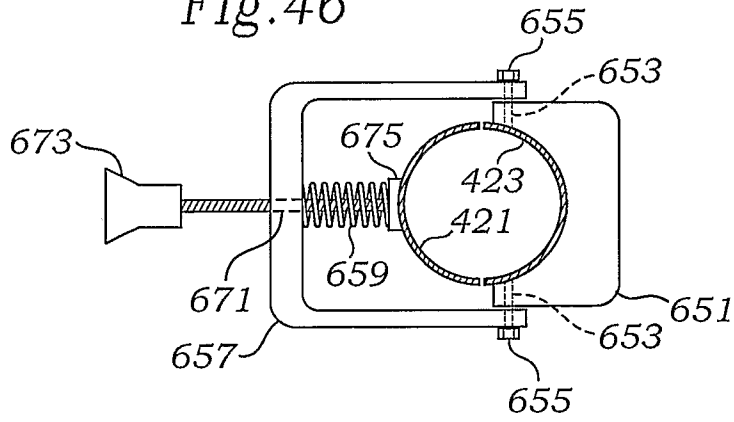


Fig.49

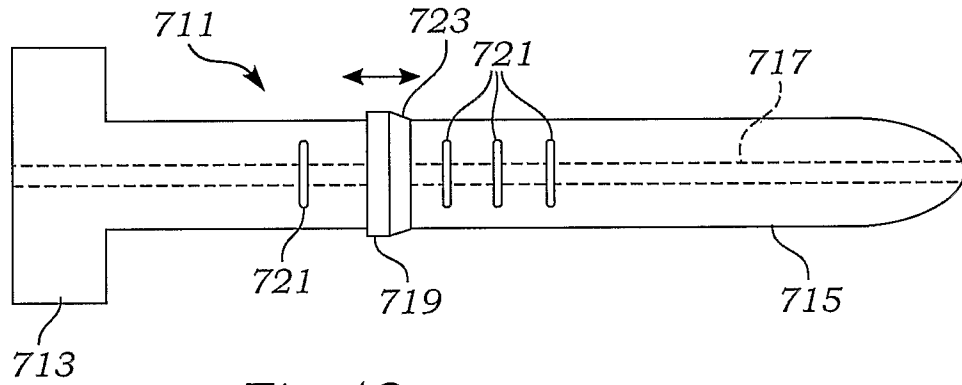


Fig.48

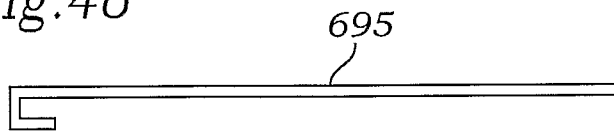
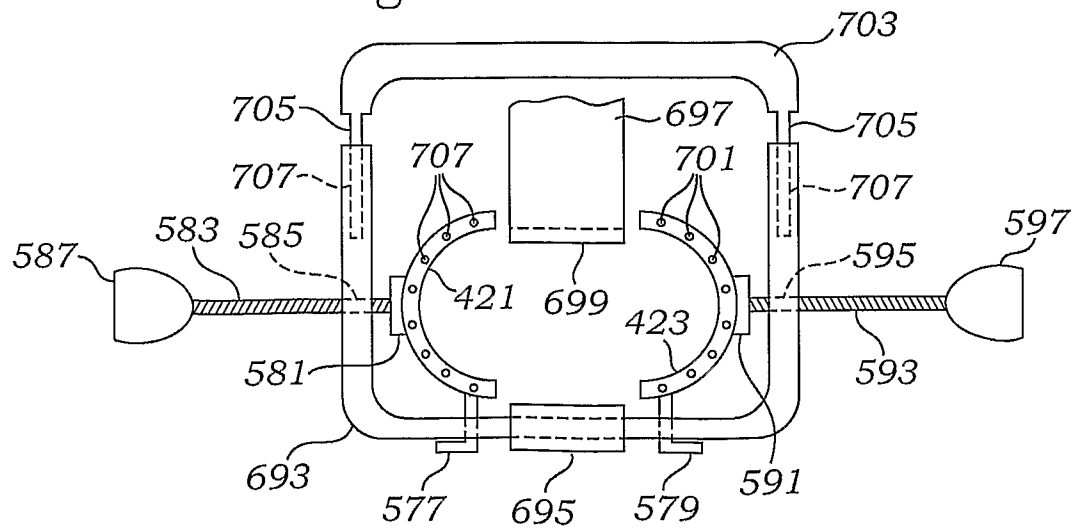


Fig.47



17/45

Fig. 50

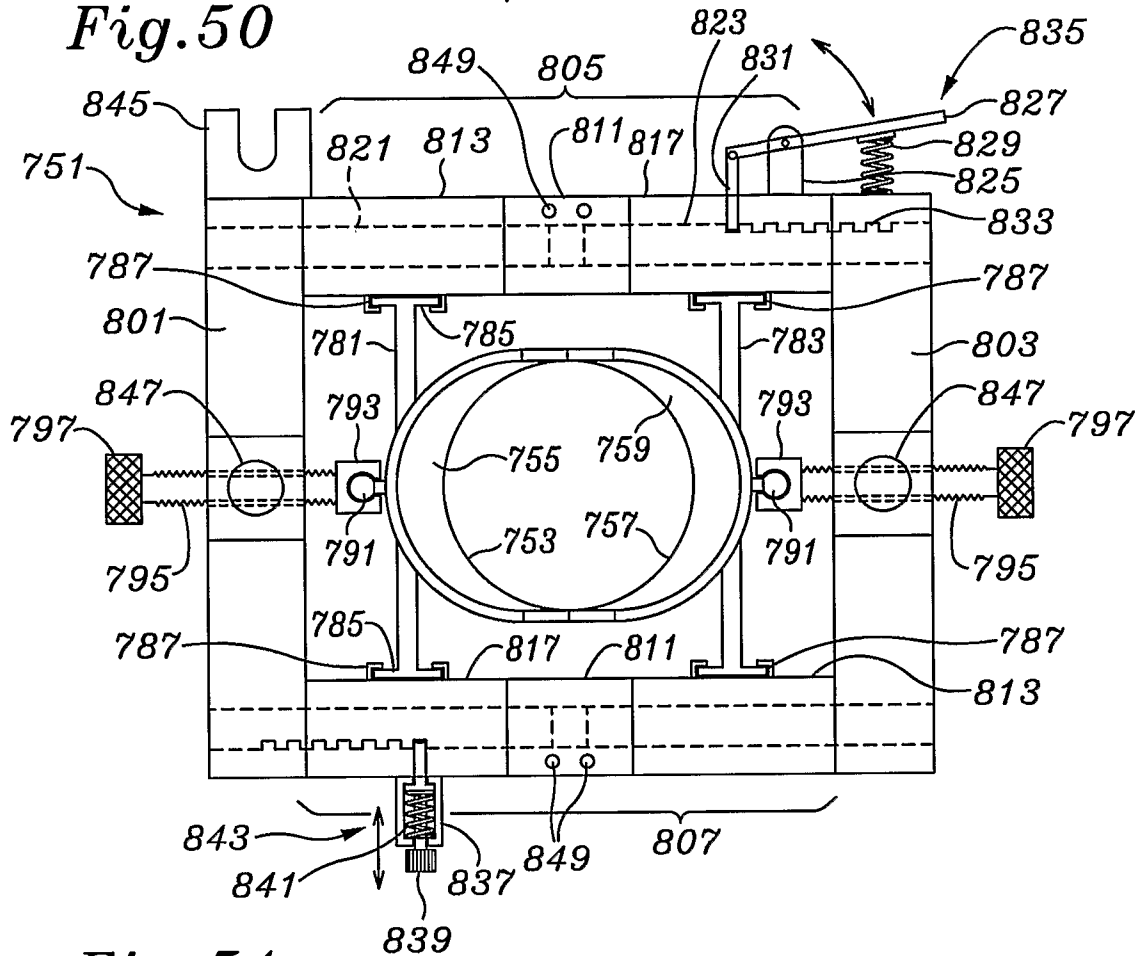
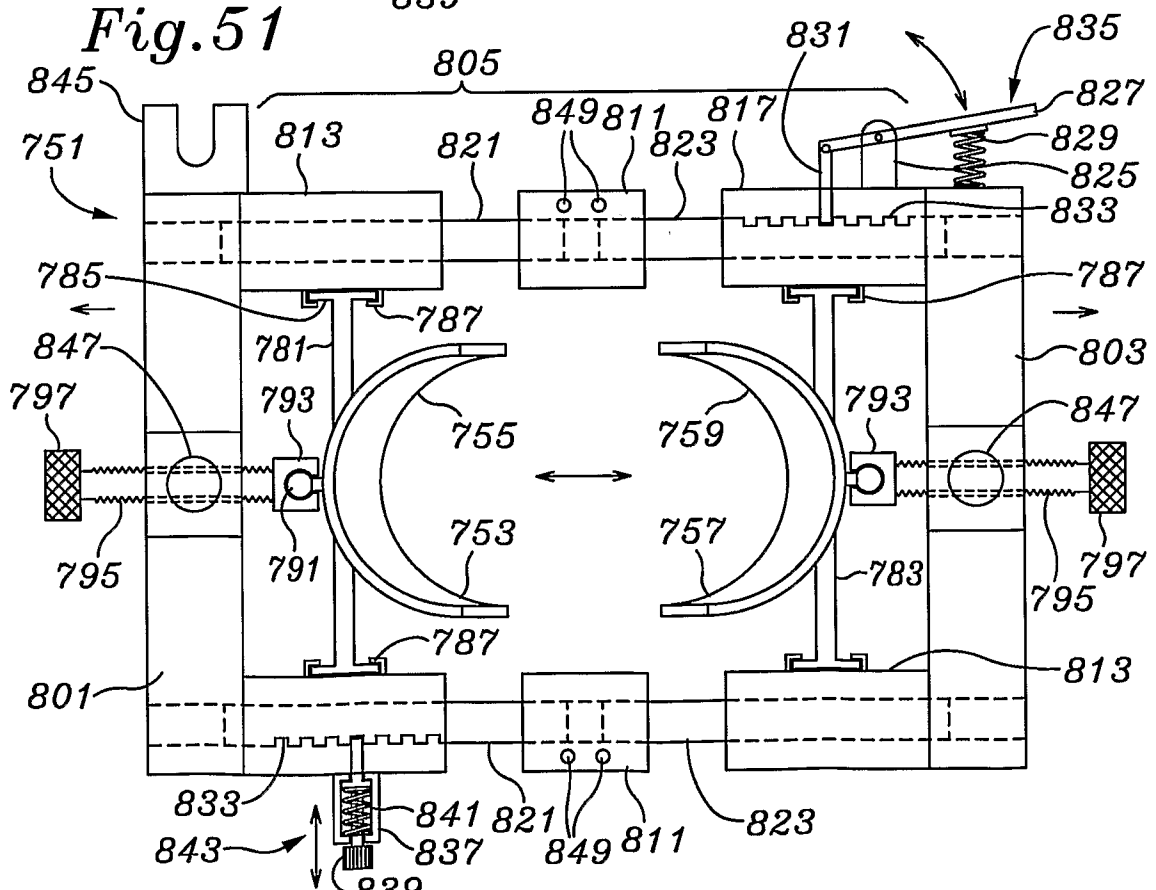


Fig. 51



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Fig. 52

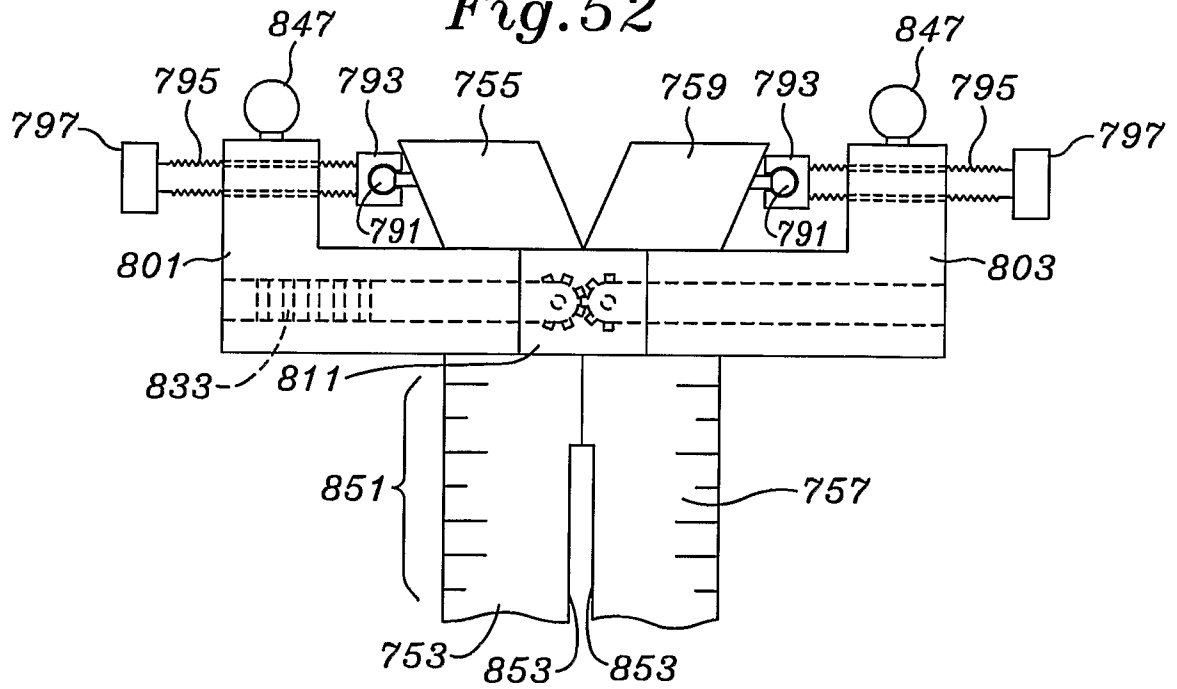


Fig. 53

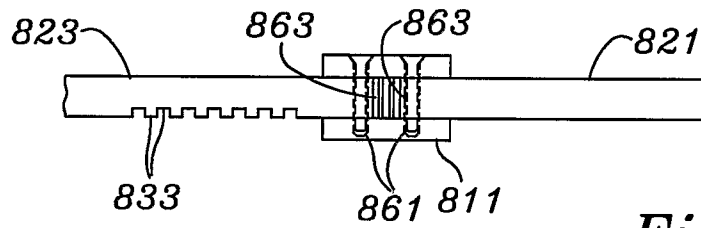


Fig. 55

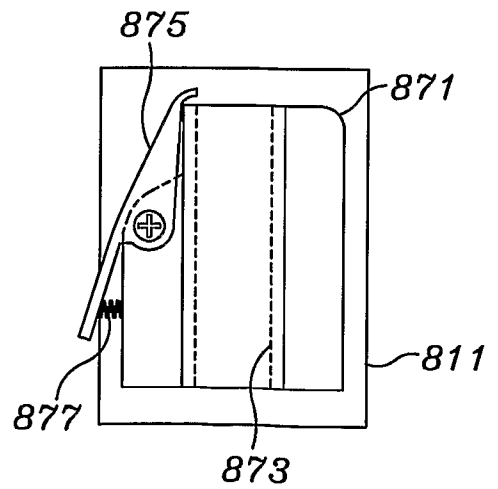
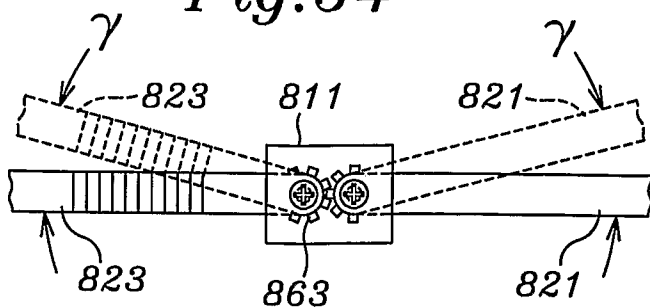


Fig. 54



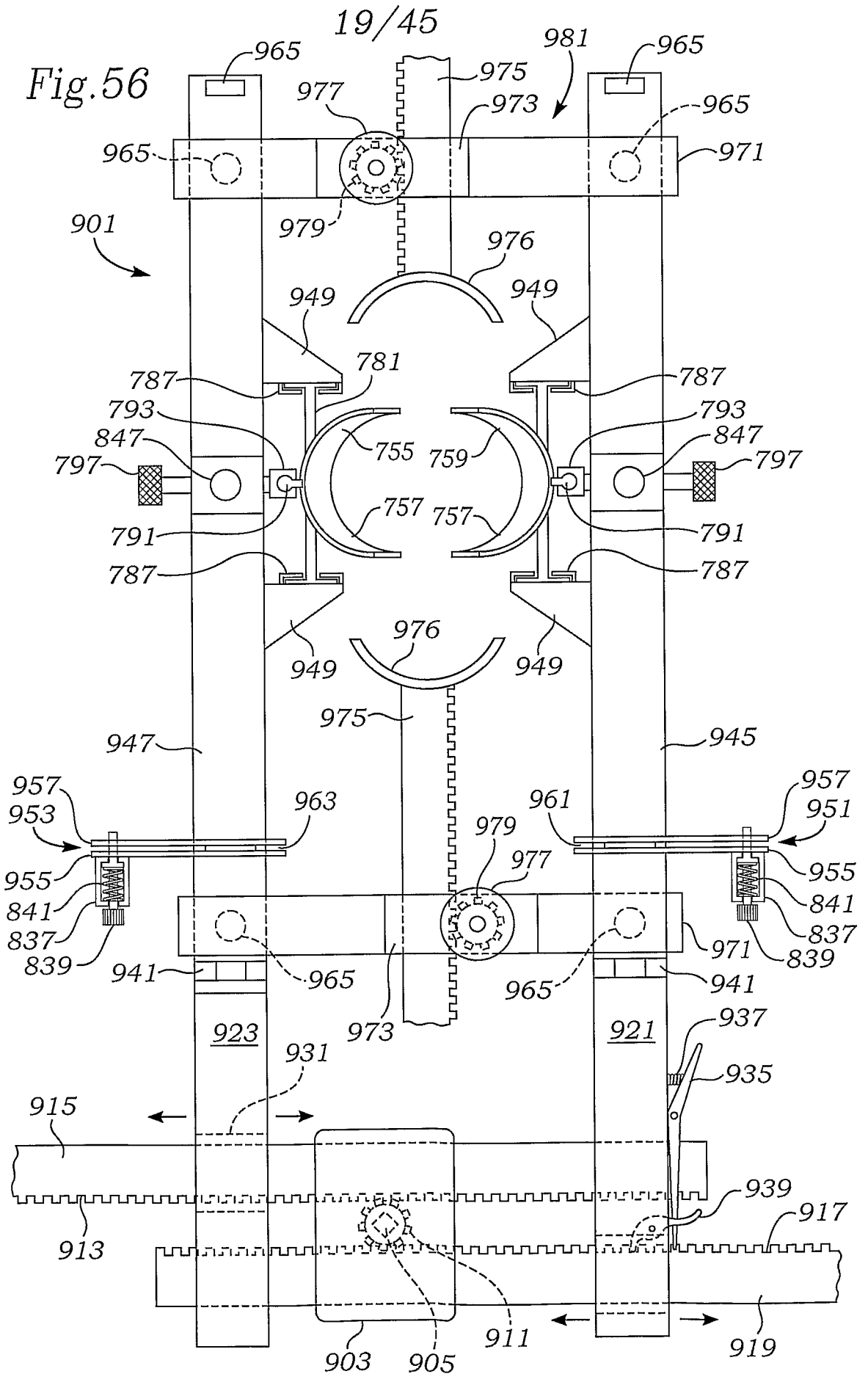


Fig.57

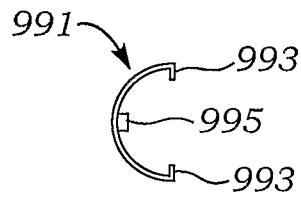


Fig.58

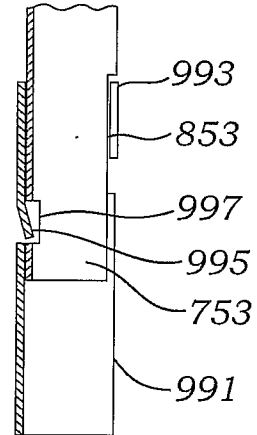


Fig.59

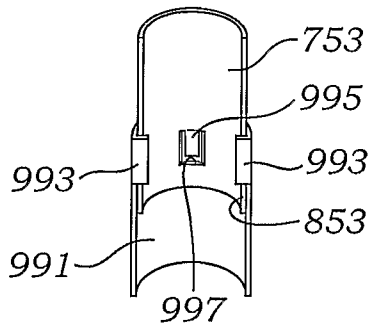
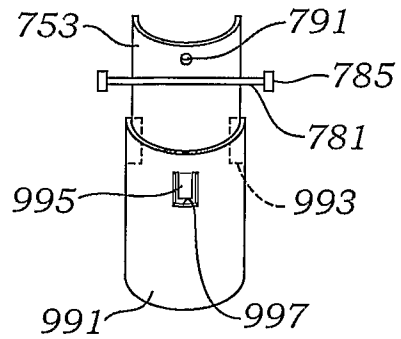


Fig.60



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Fig. 62

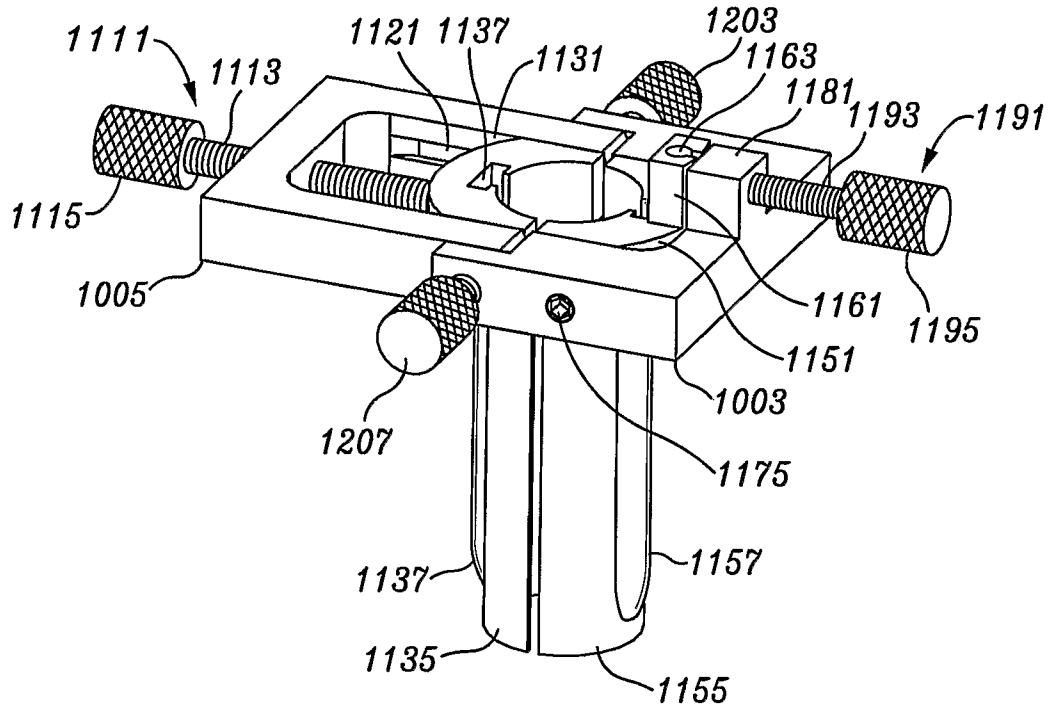


Fig. 63

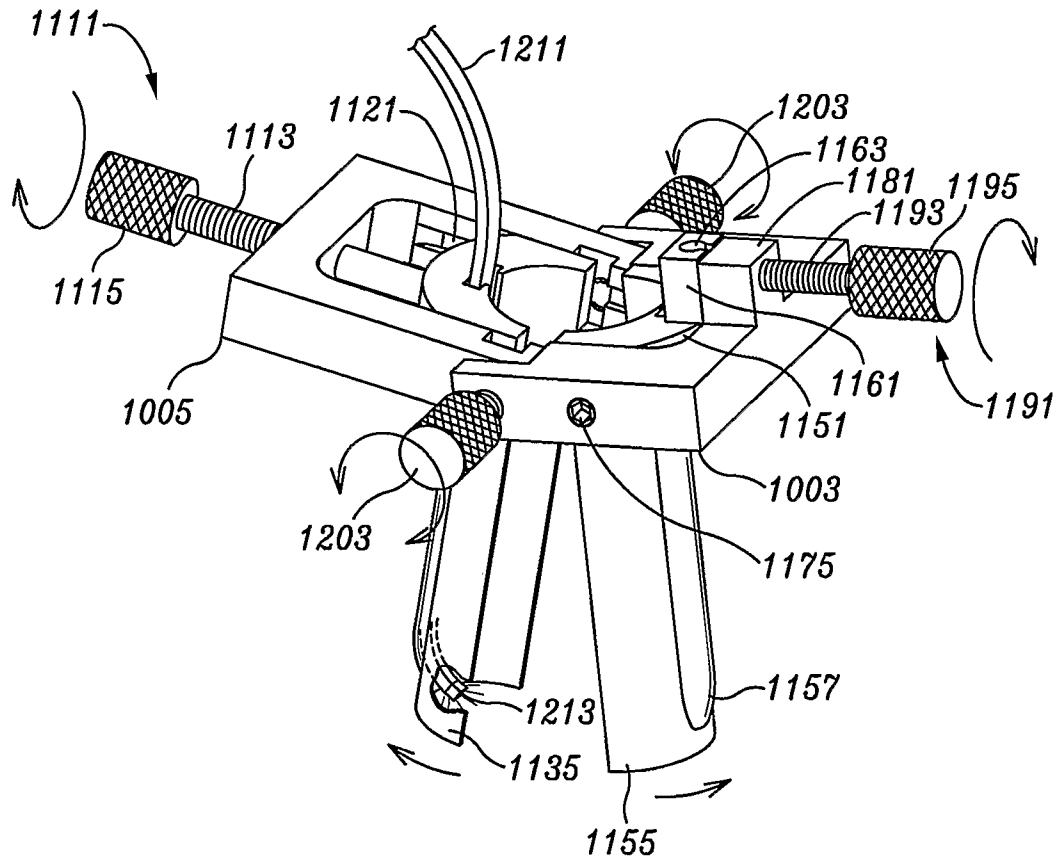


Fig. 64

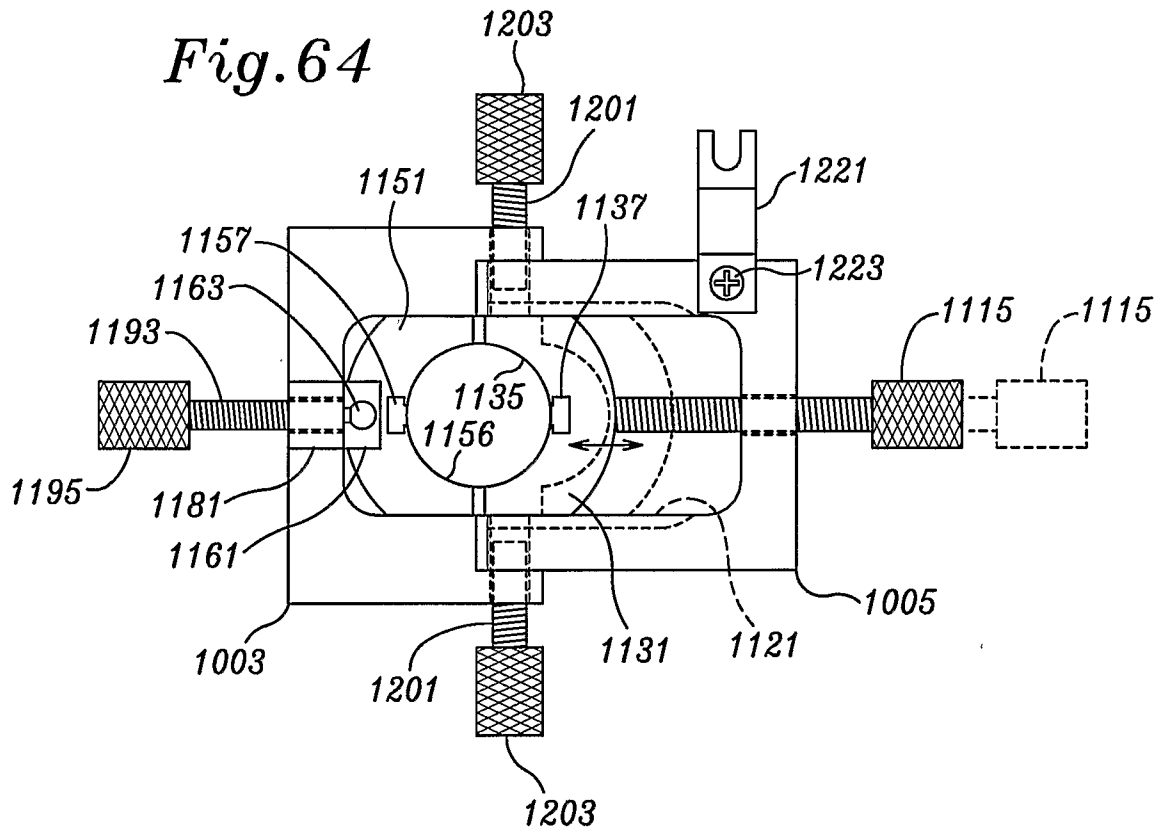


Fig. 65

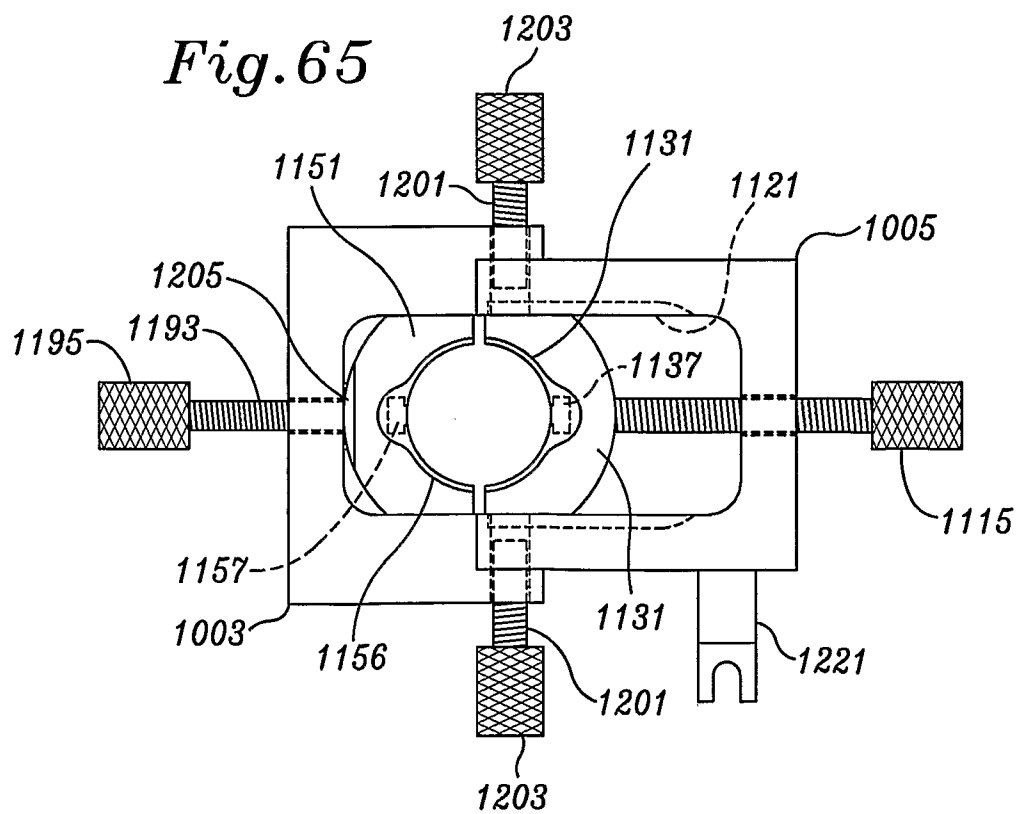
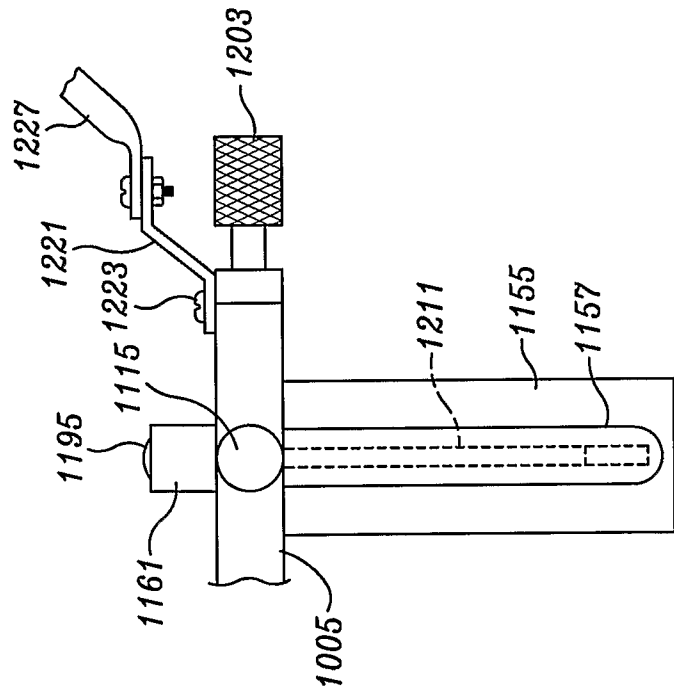


Fig. 66



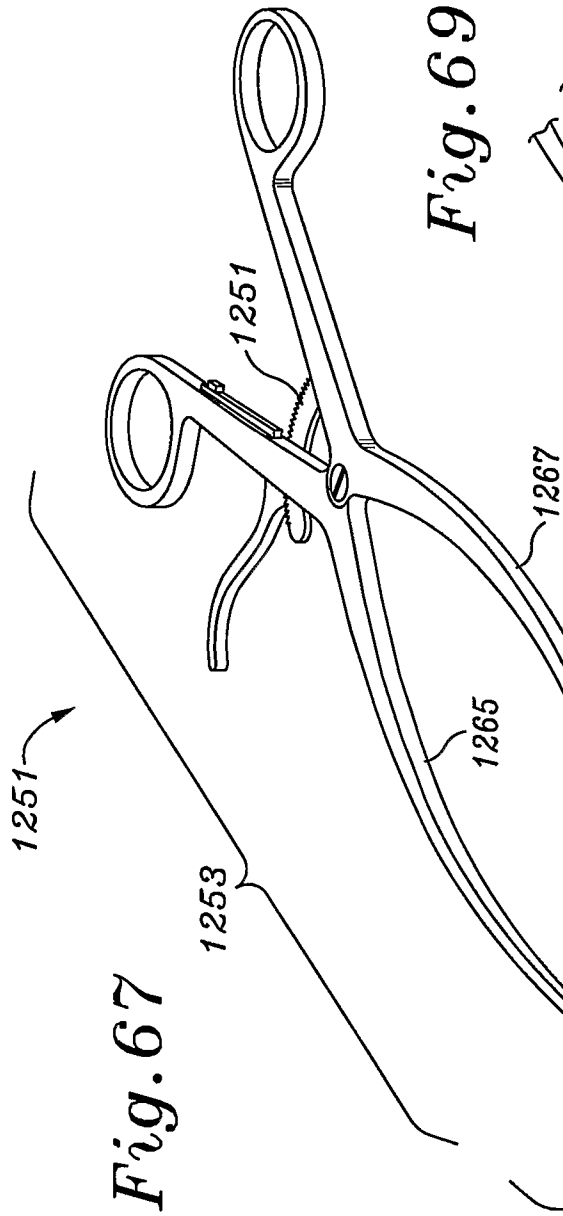


Fig. 69

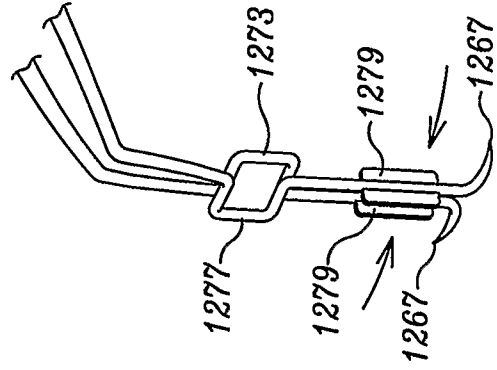


Fig. 68

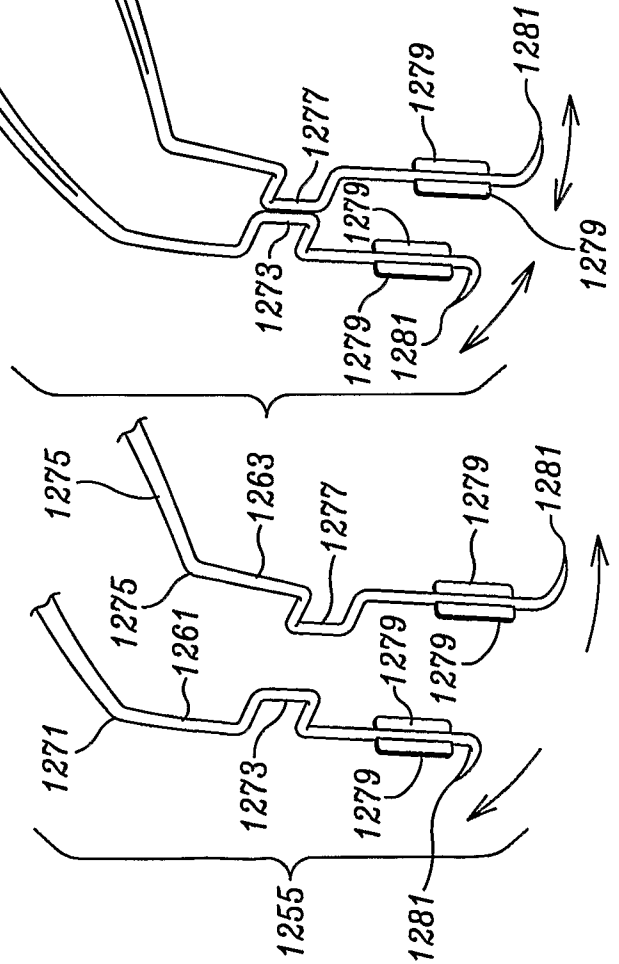


Fig. 70

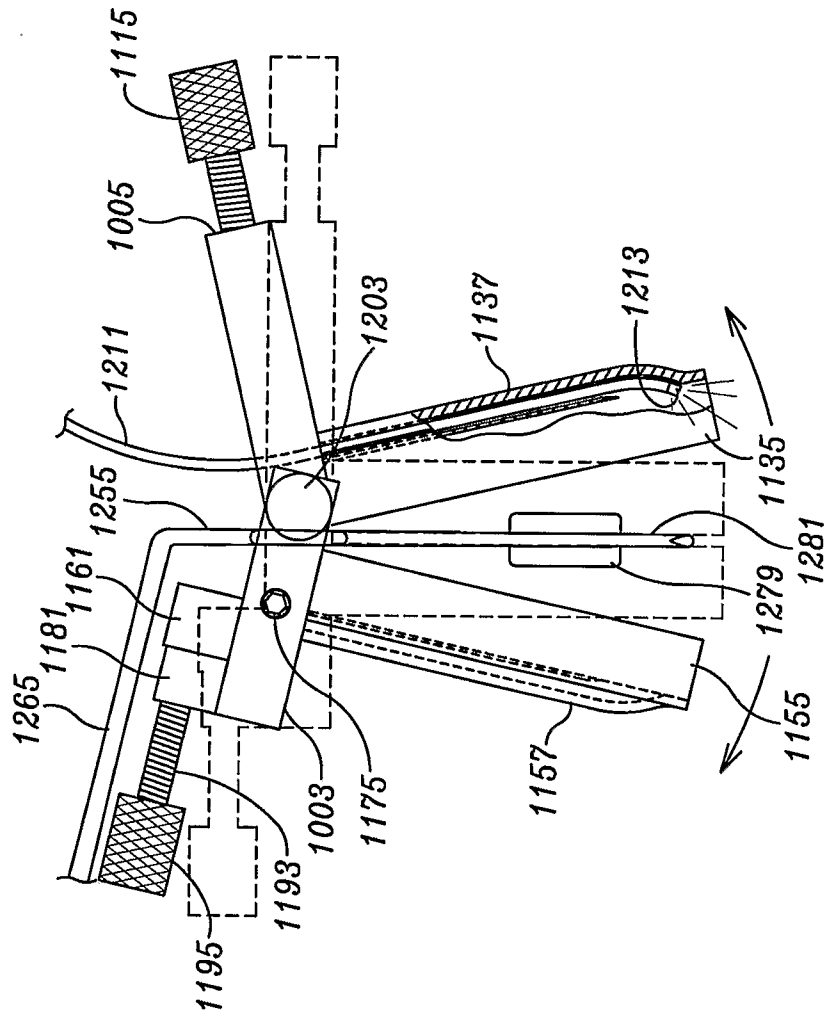


Fig. 72

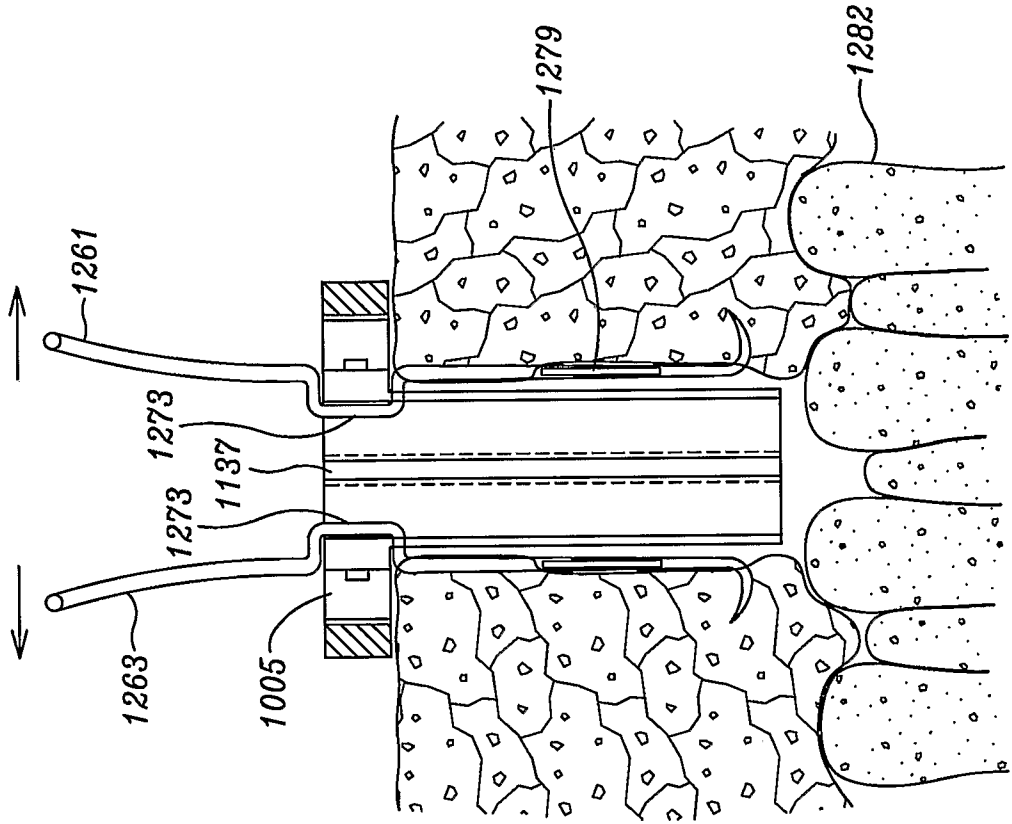


Fig. 71

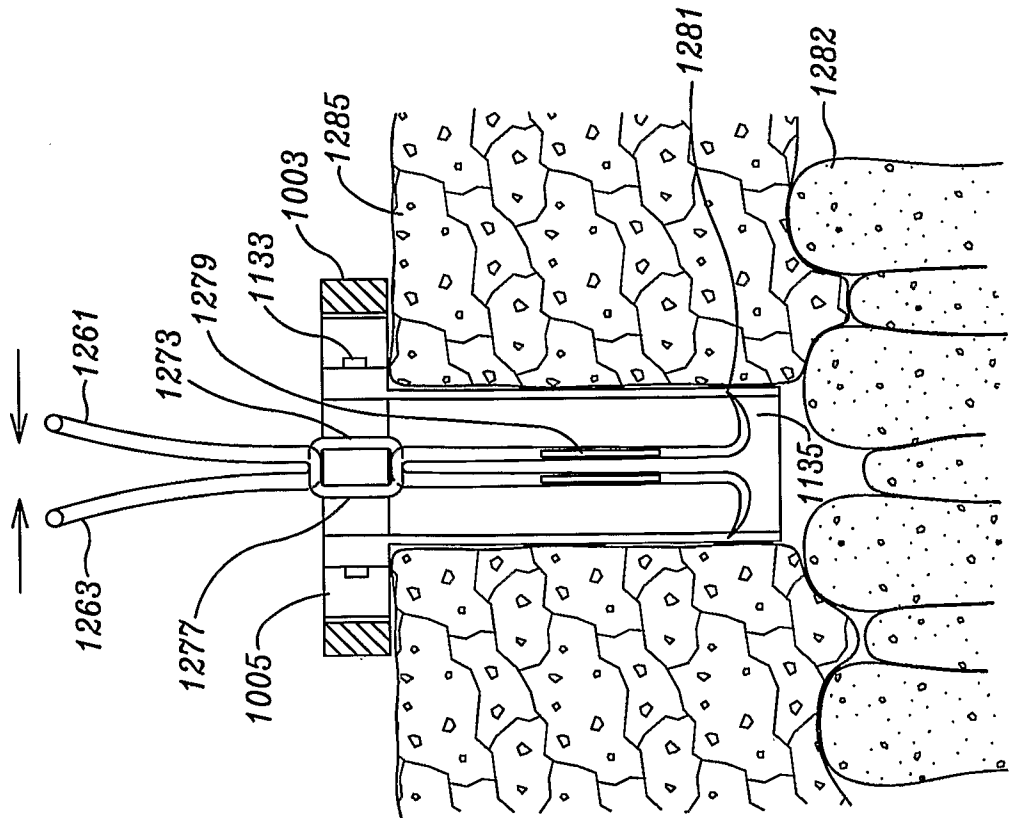


Fig. 73

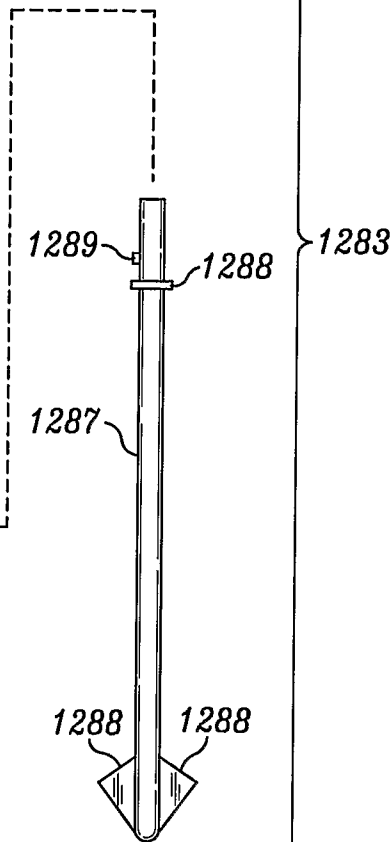
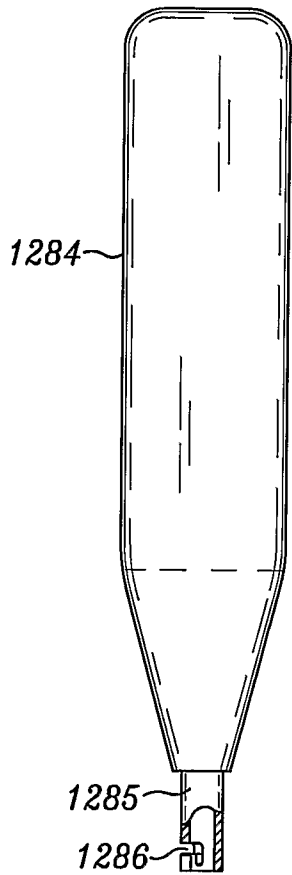


Fig. 74

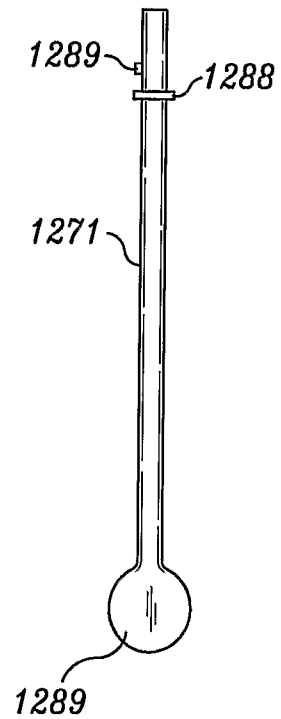


Fig. 75

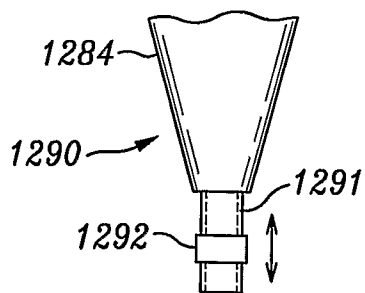
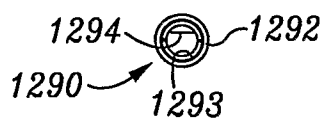


Fig. 76



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Fig. 77

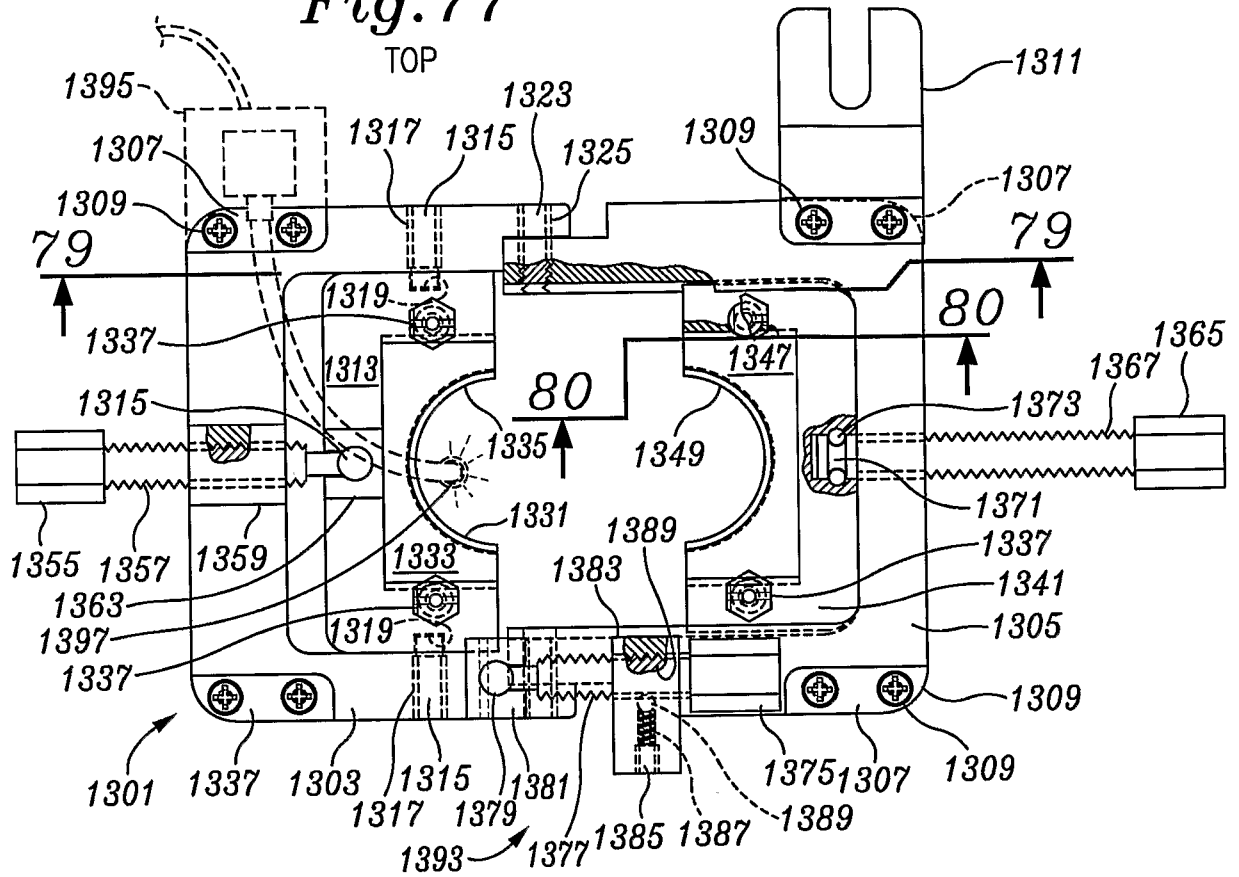


Fig. 78

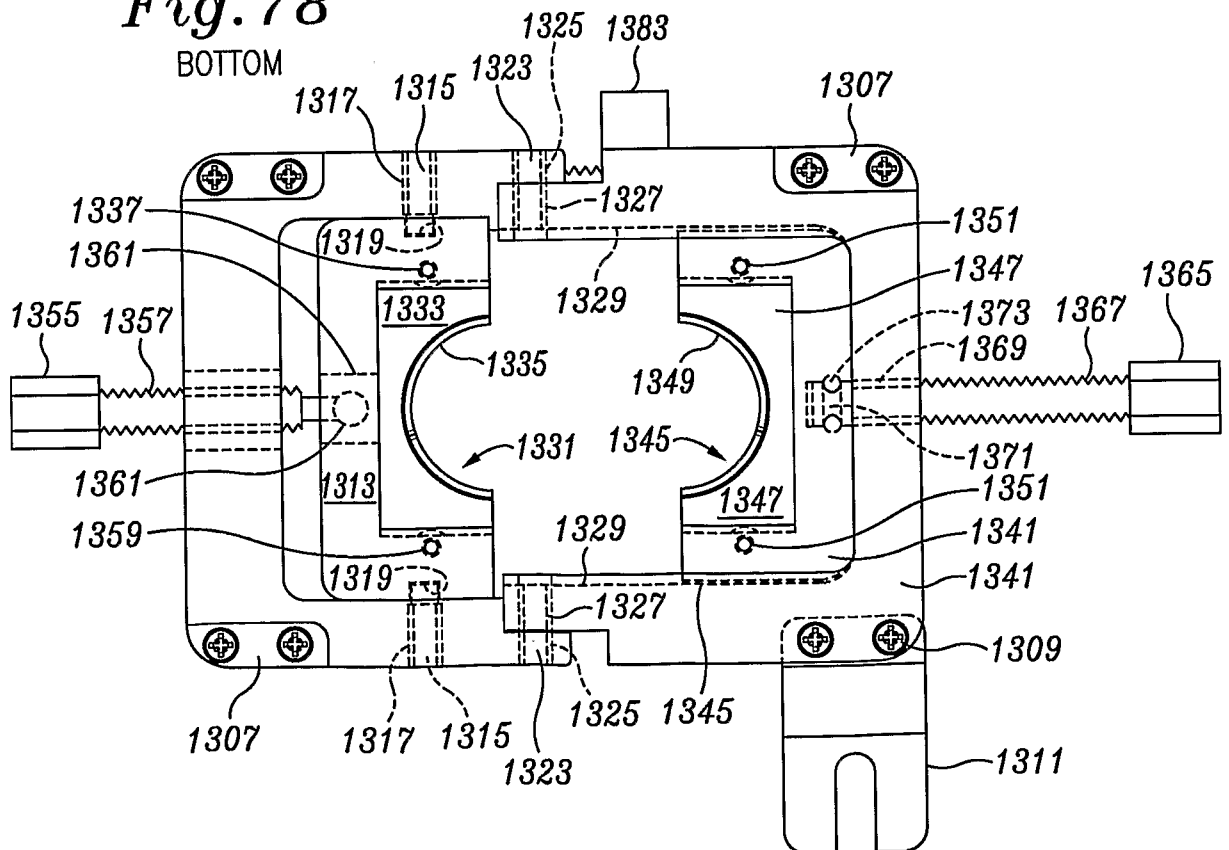


Fig. 79

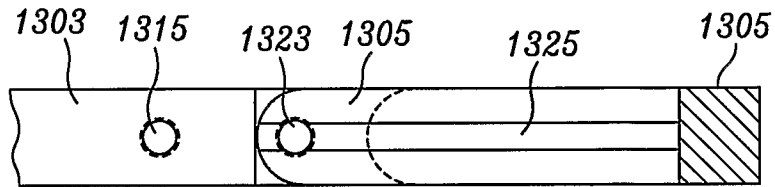


Fig. 80

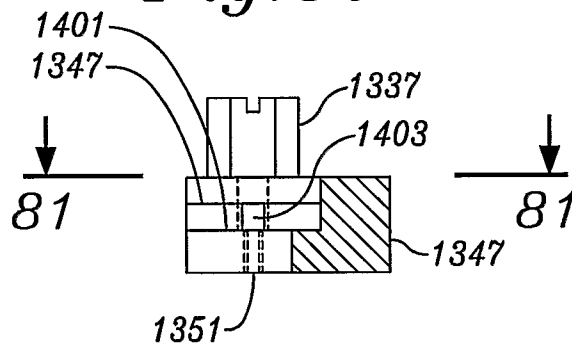


Fig. 81

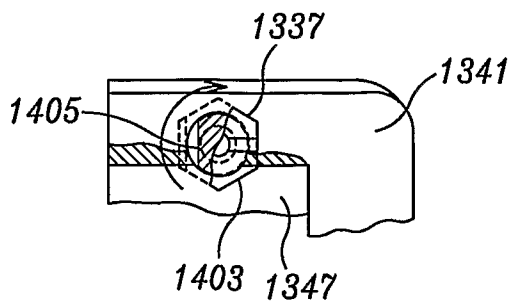


Fig. 82

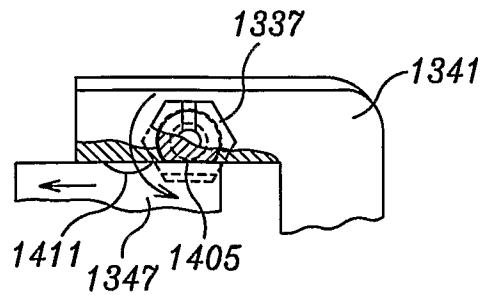


Fig. 88

TOP LEFT

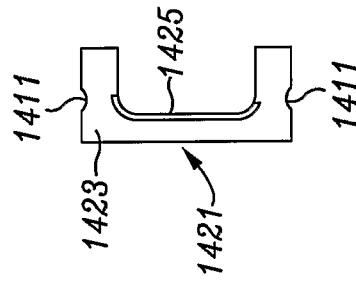


Fig. 89

TOP RIGHT

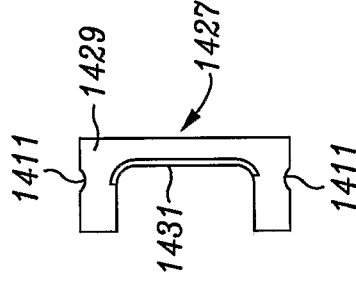


Fig. 83

TOP LEFT

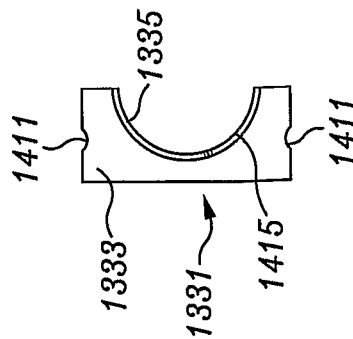


Fig. 84

TOP RIGHT

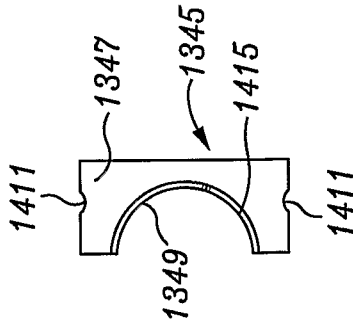


Fig. 85

LEFT SIDE

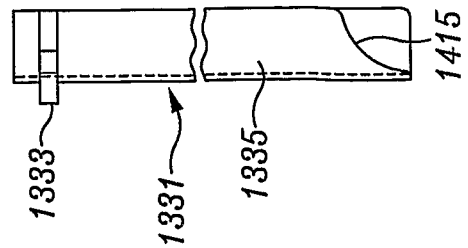


Fig. 86

RIGHT SIDE

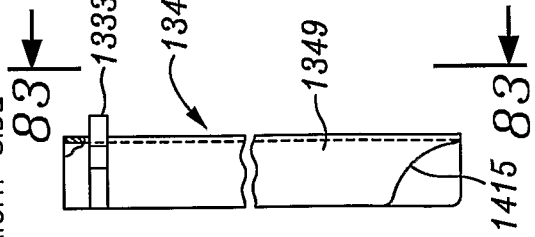


Fig. 87

REAR

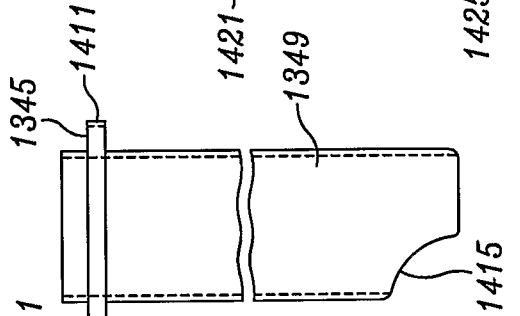


Fig. 90

LEFT SIDE

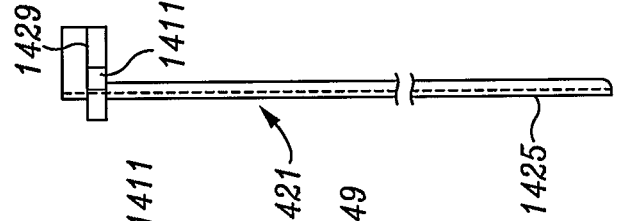


Fig. 91

RIGHT SIDE

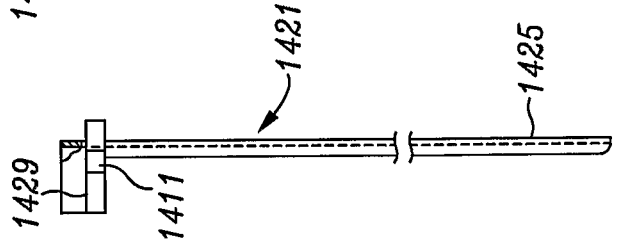
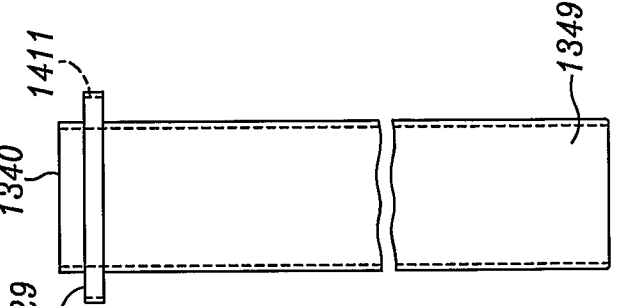


Fig. 92

REAR



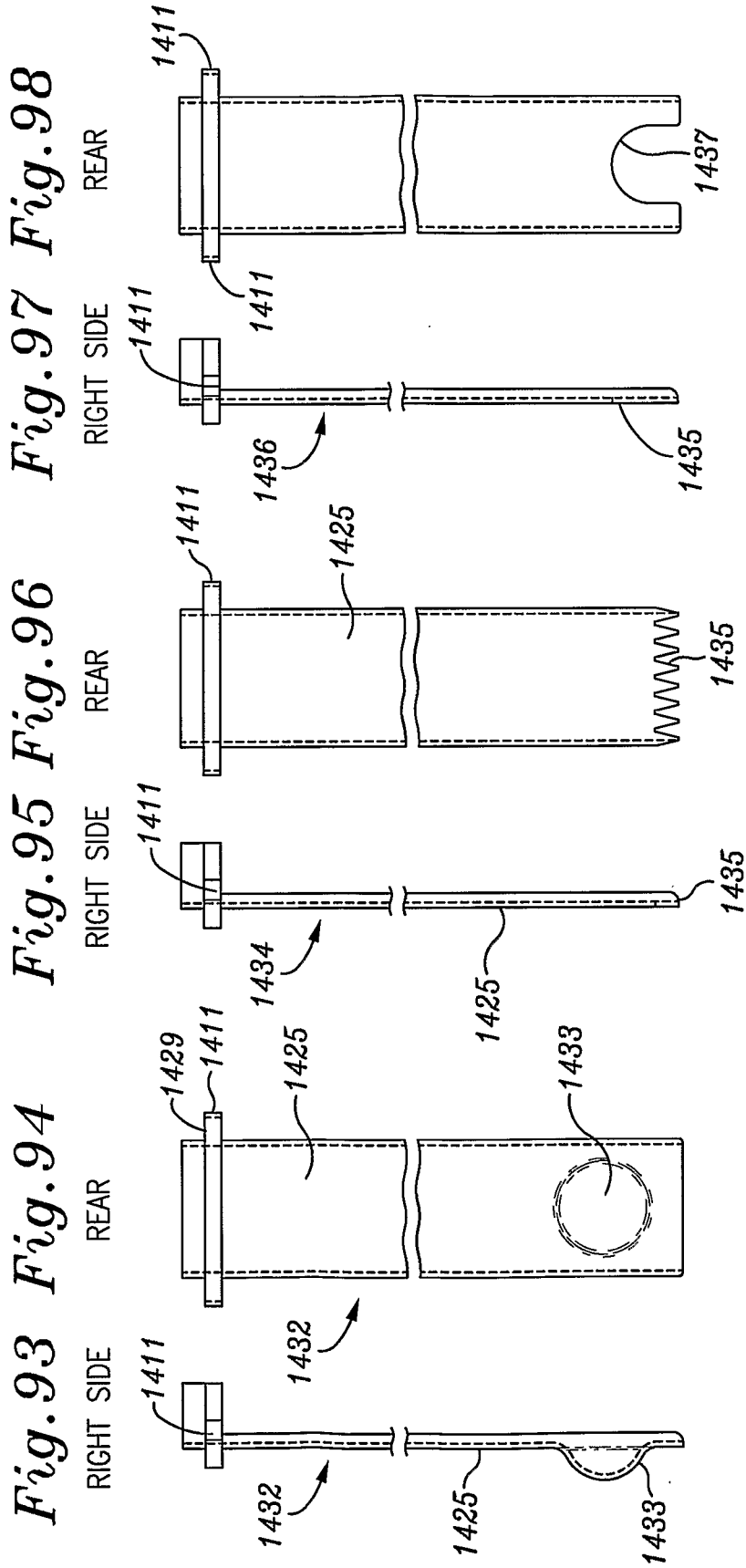
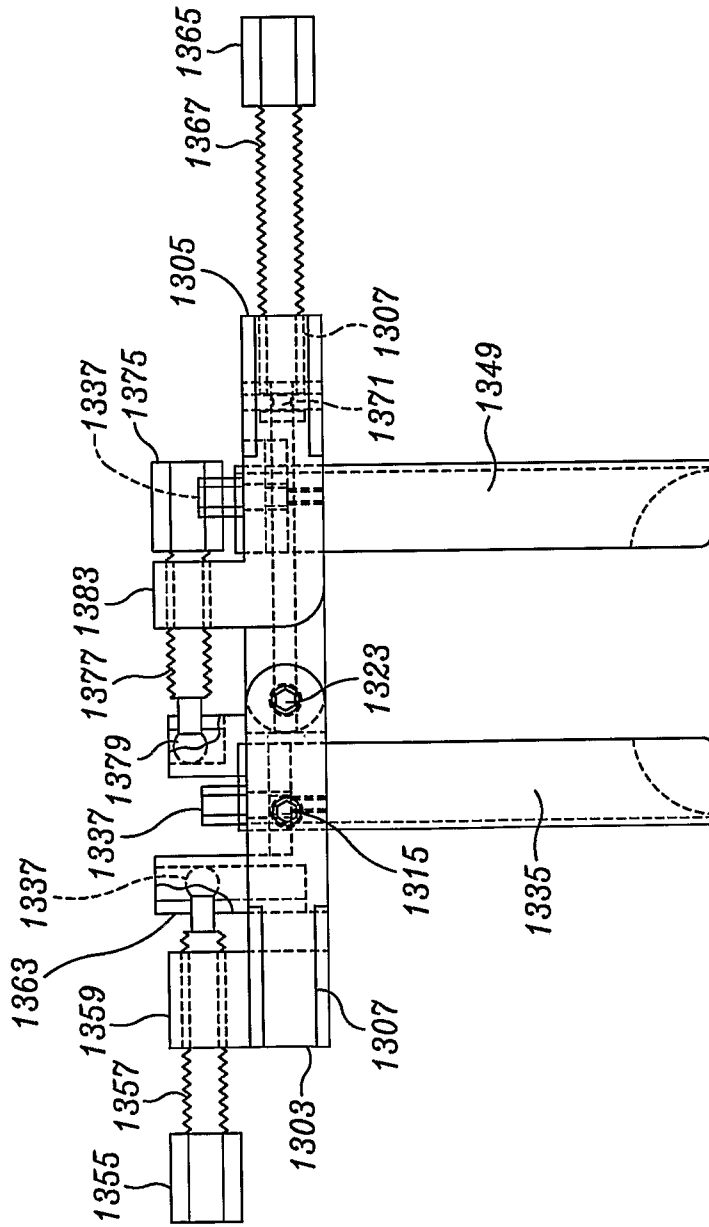


Fig. 99
LEFT SIDE



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Fig. 100

RIGHT SIDE

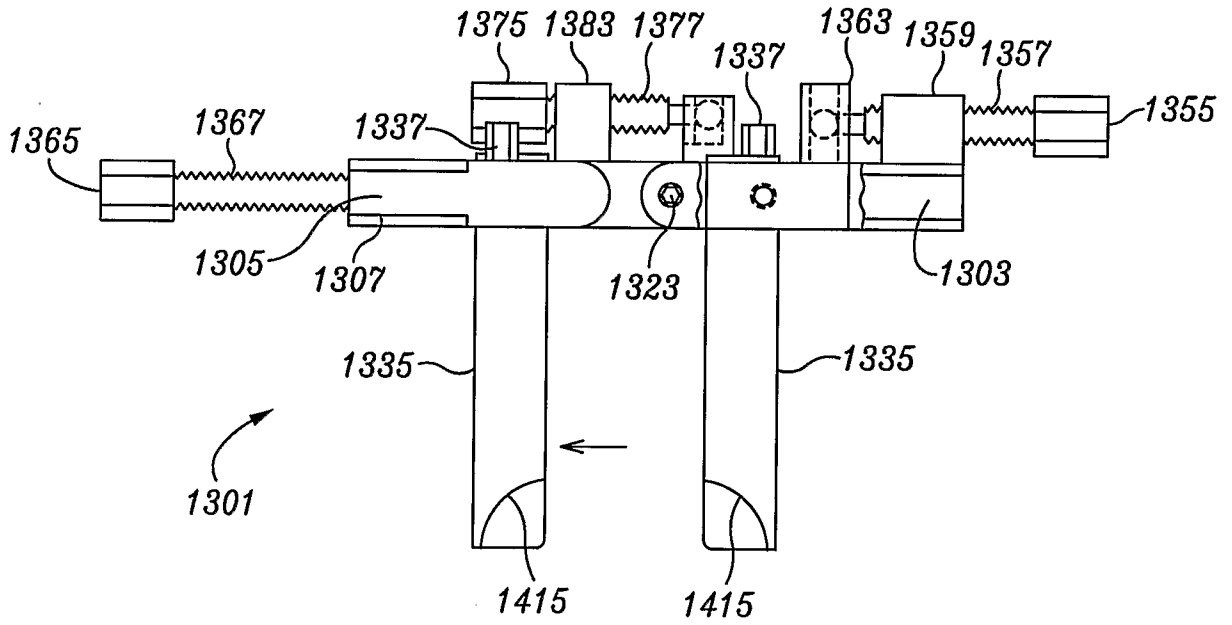
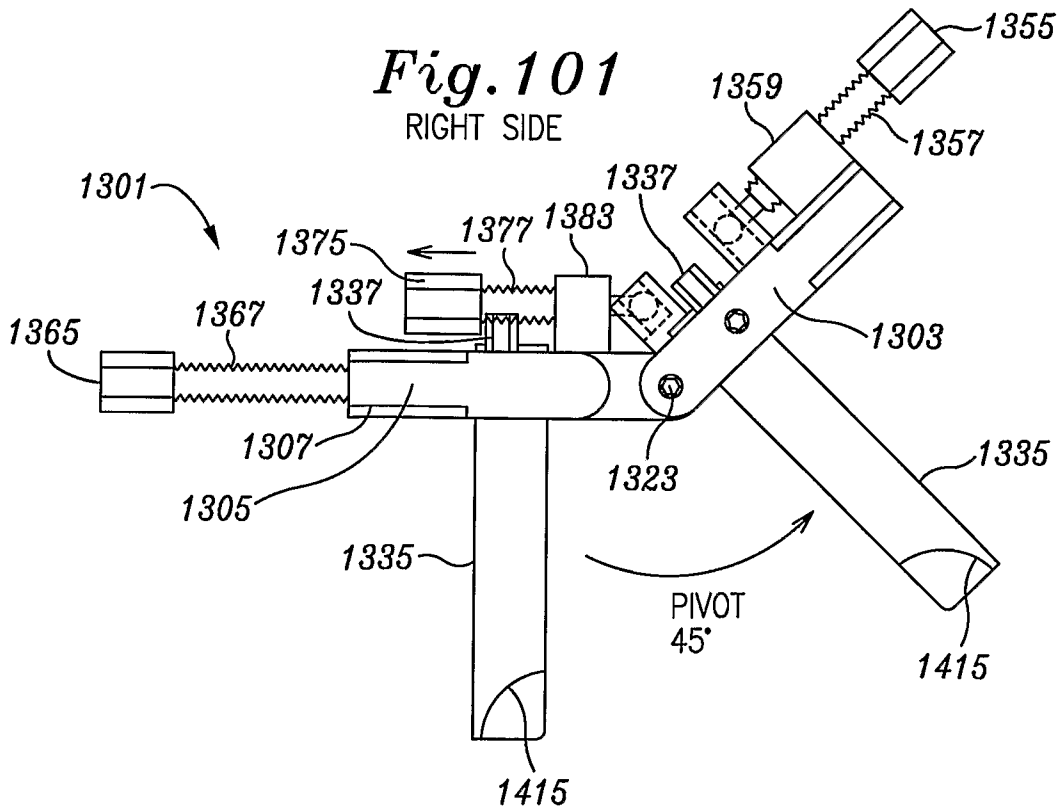


Fig. 101

RIGHT SIDE



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Fig. 102

RIGHT SIDE

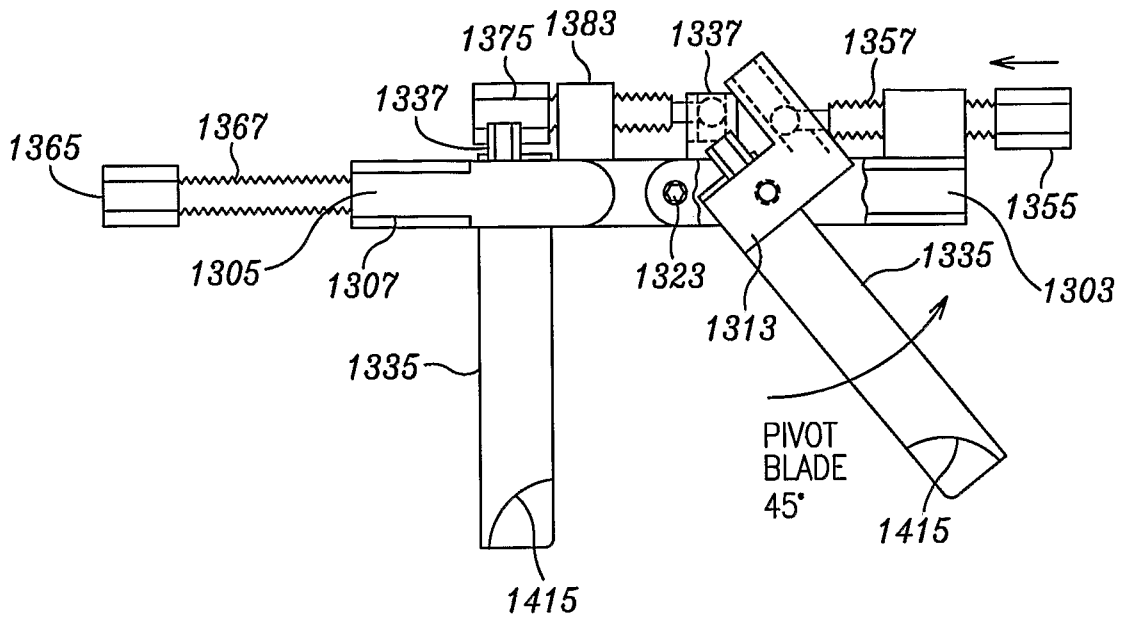
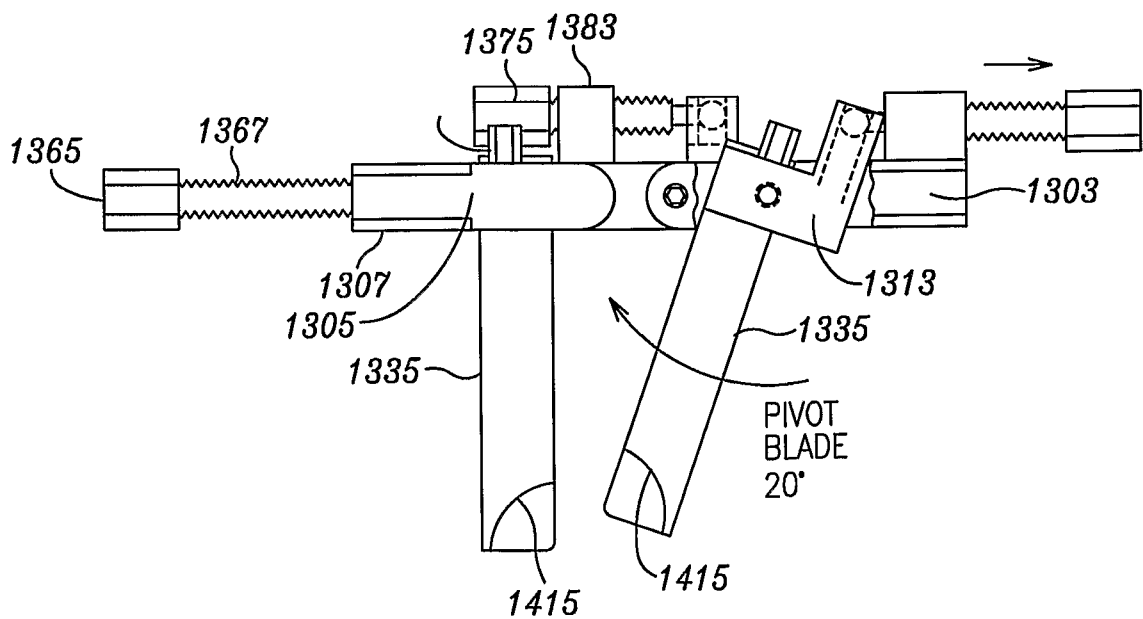


Fig. 103

RIGHT SIDE



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Fig. 104

RIGHT SIDE

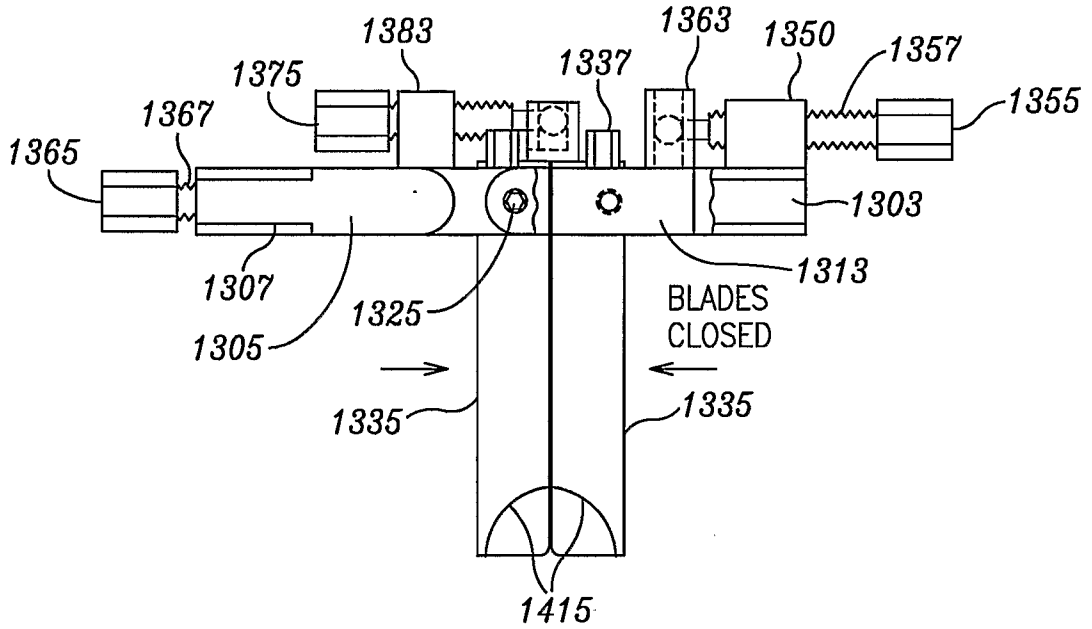
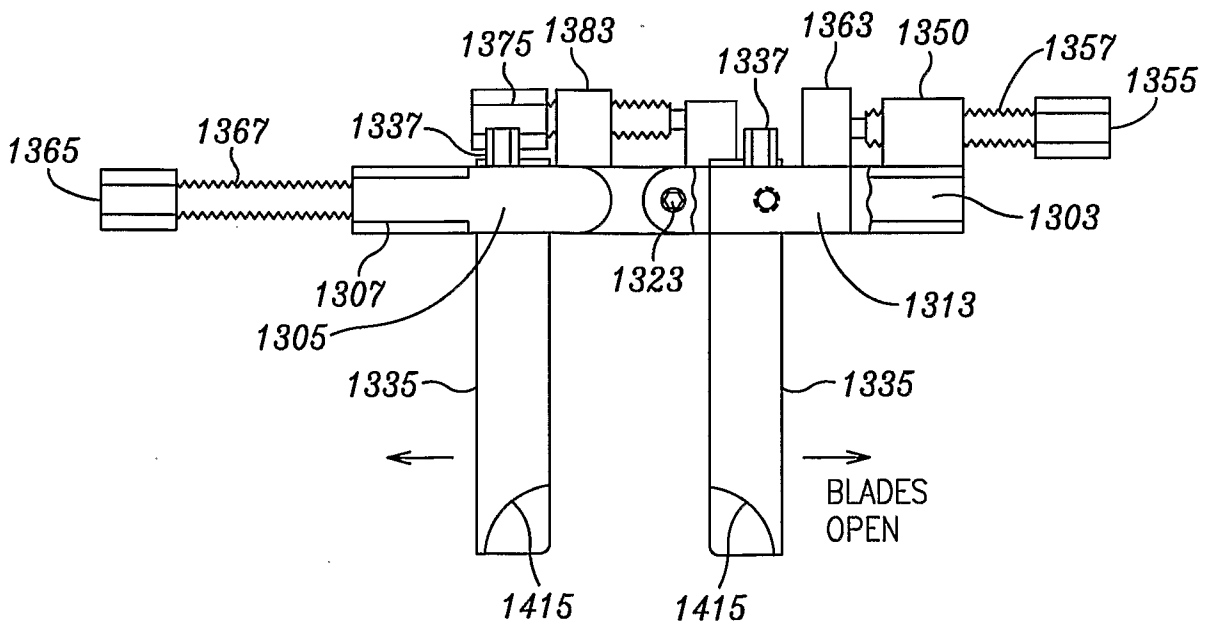


Fig. 105

RIGHT SIDE



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Fig. 106

TOP

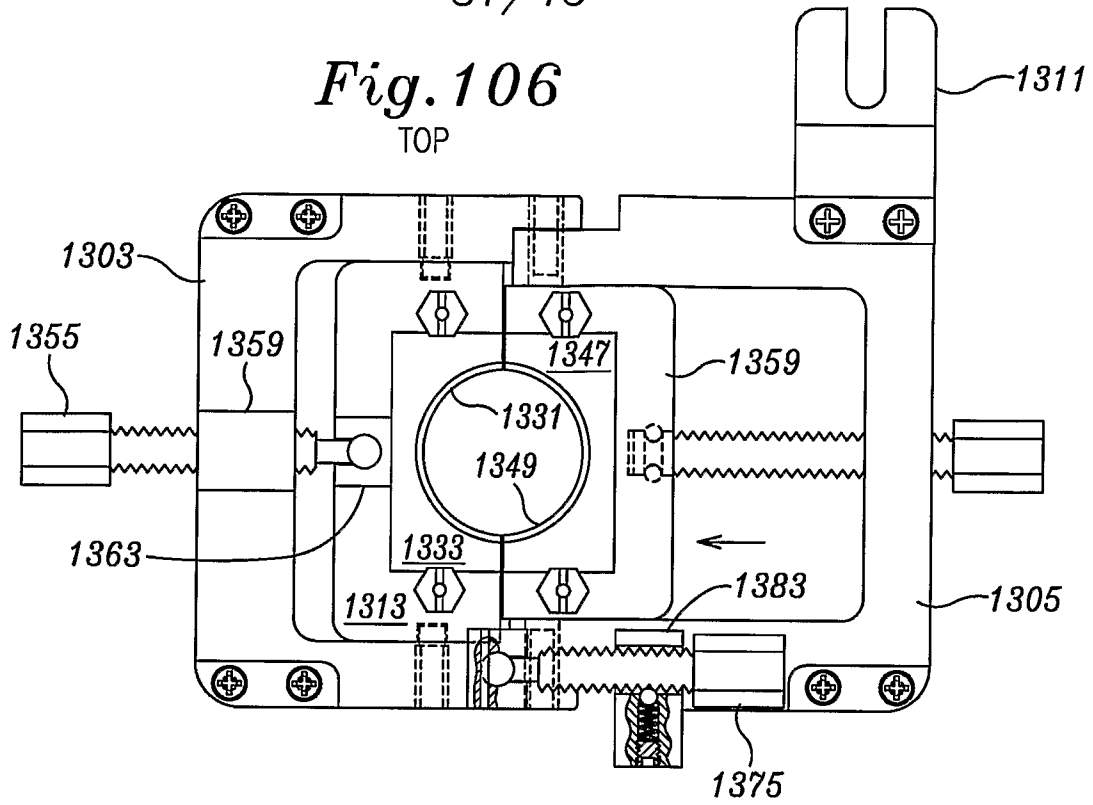


Fig. 107

LEFT SIDE

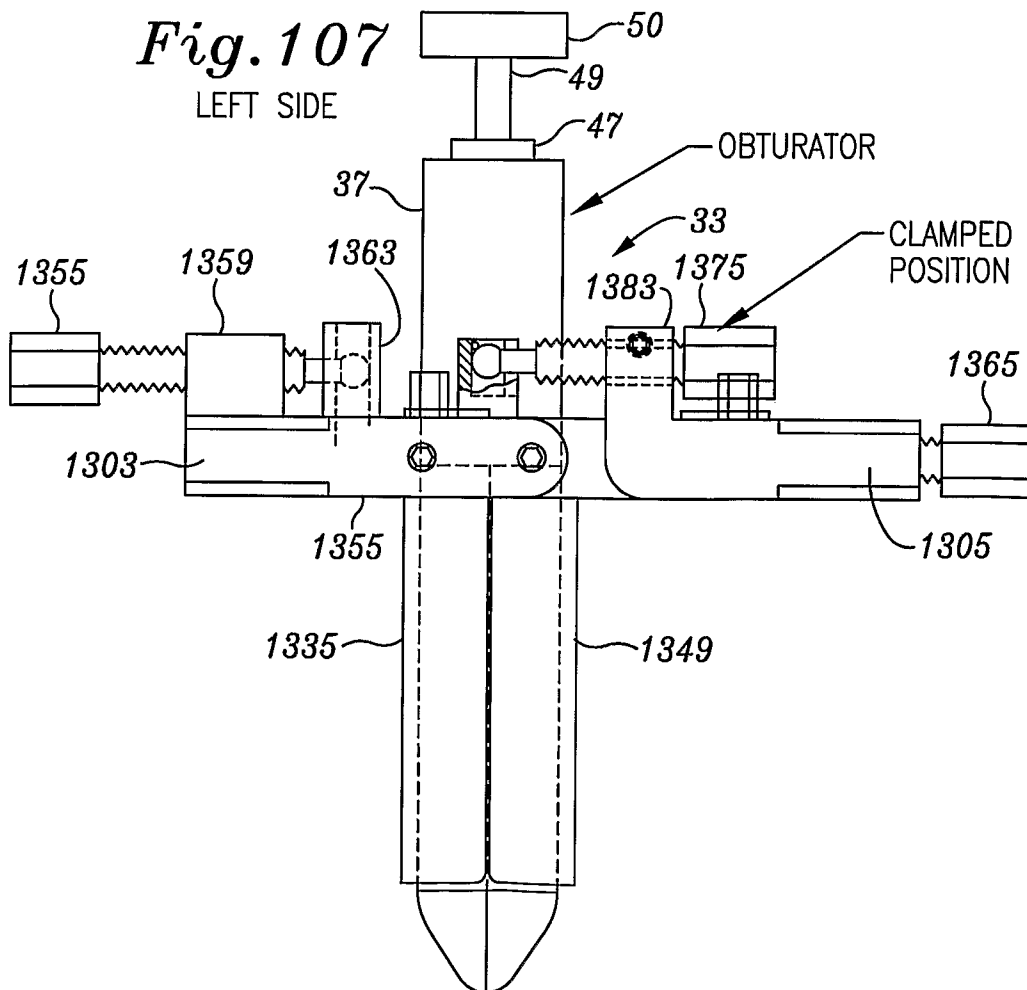
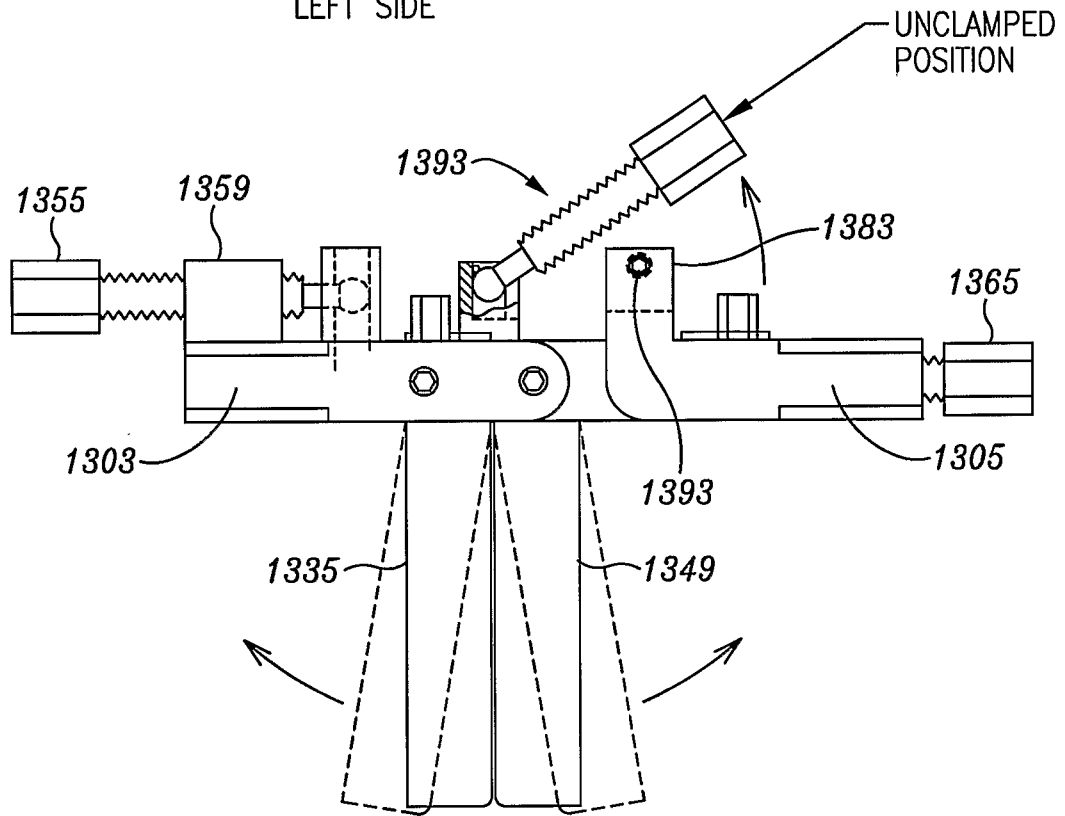
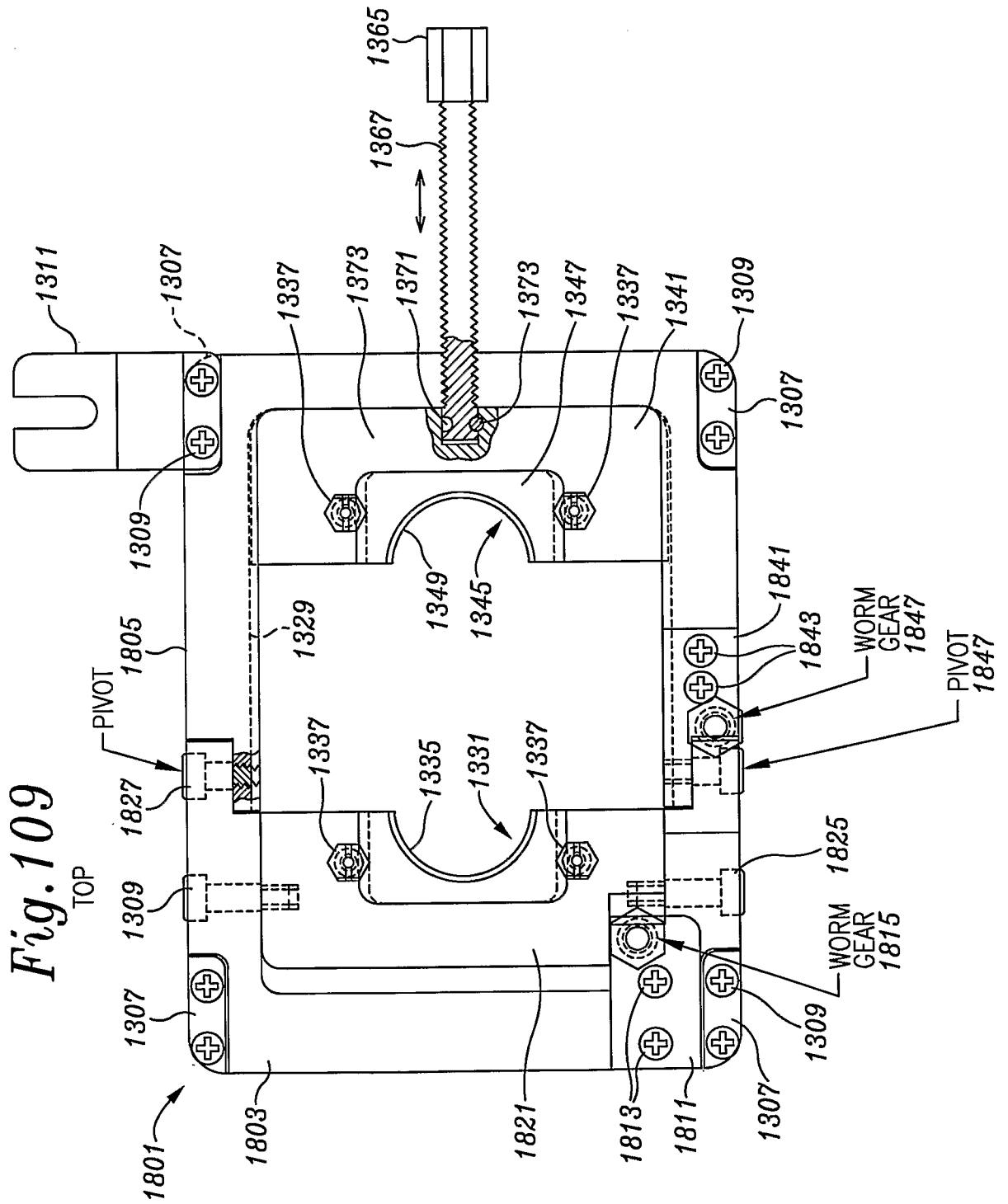


Fig. 108

LEFT SIDE





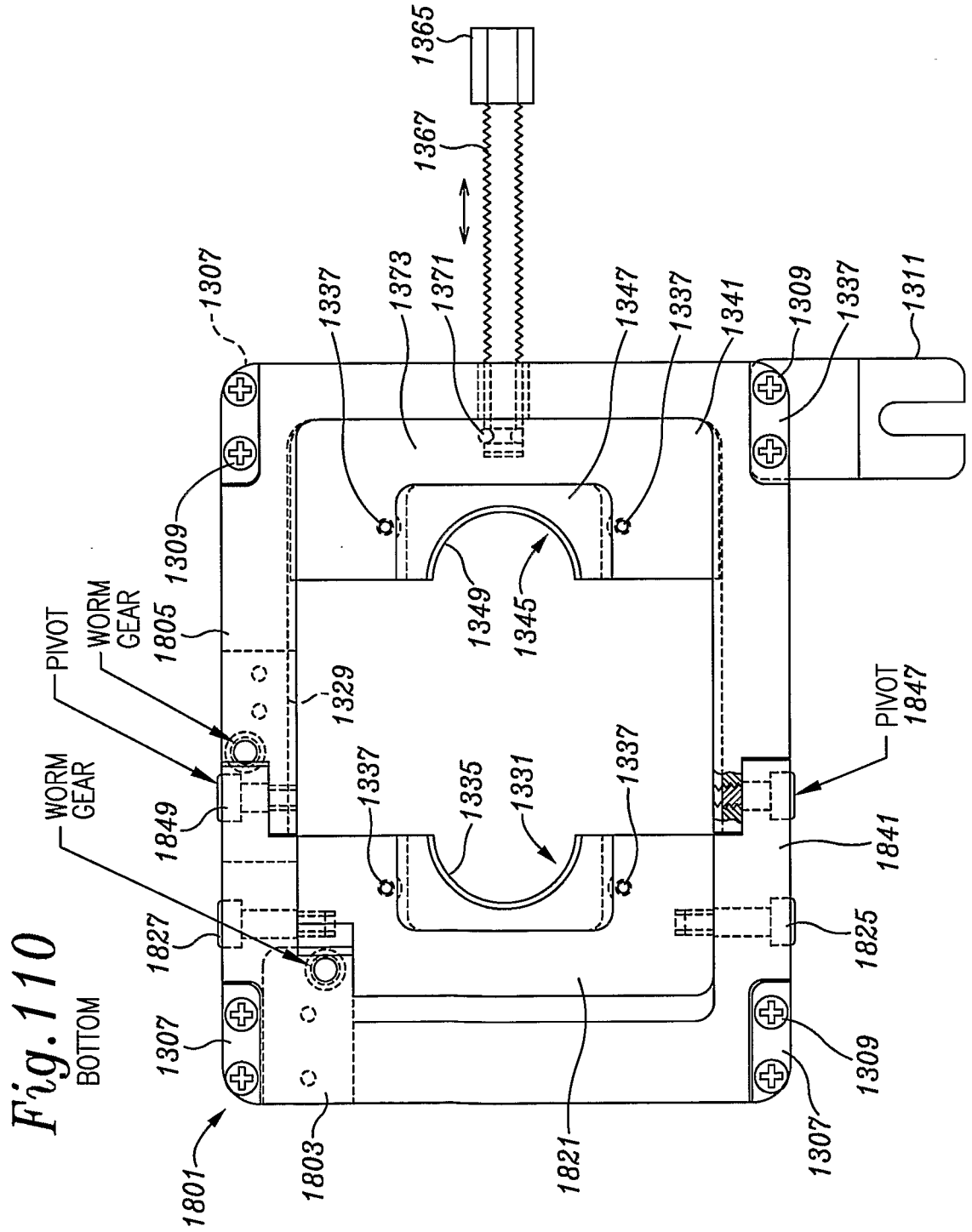
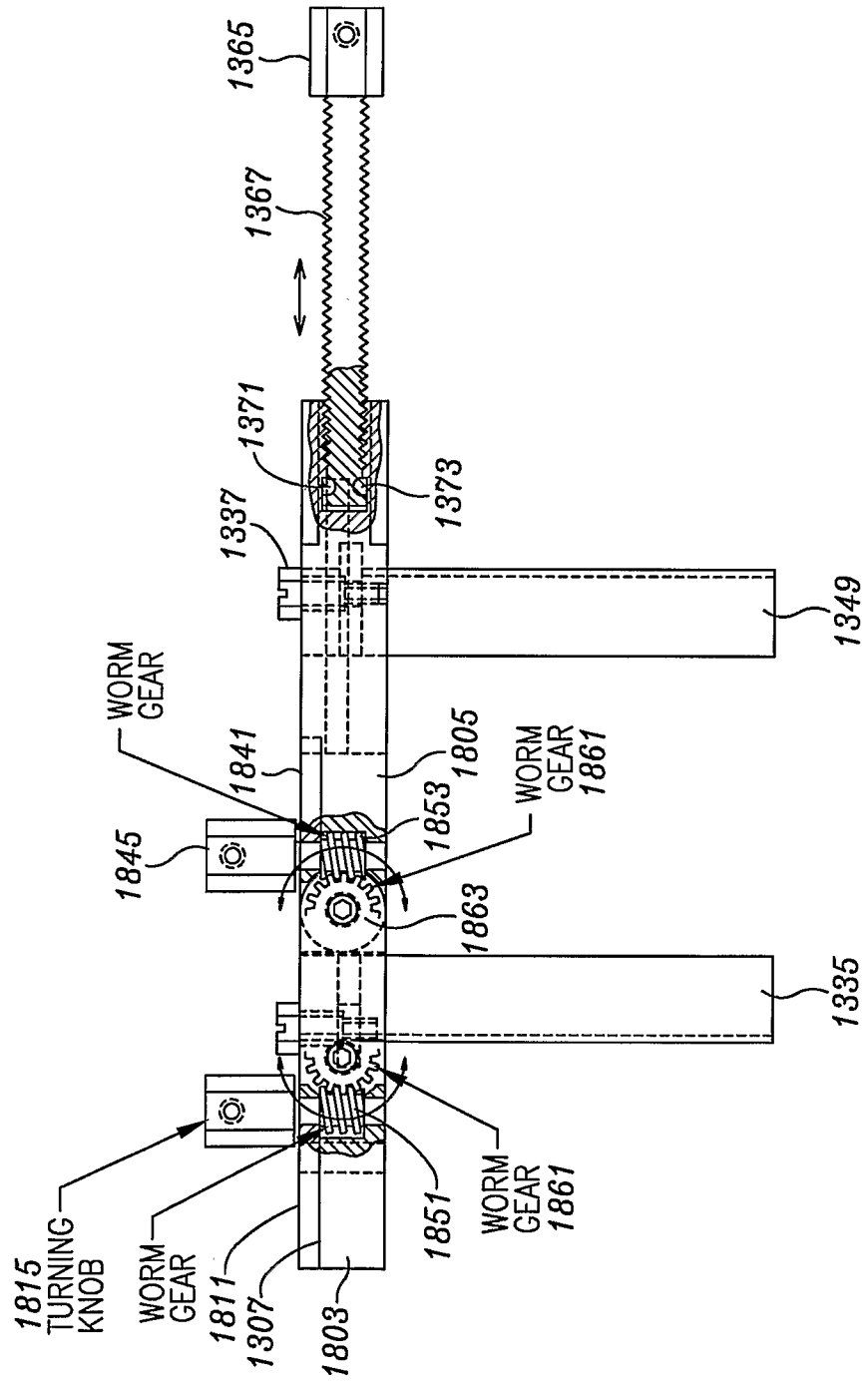


Fig. 111
PARTIALLY BROKEN AWAY
LEFT SIDE



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Fig. 112

LEFT SIDE

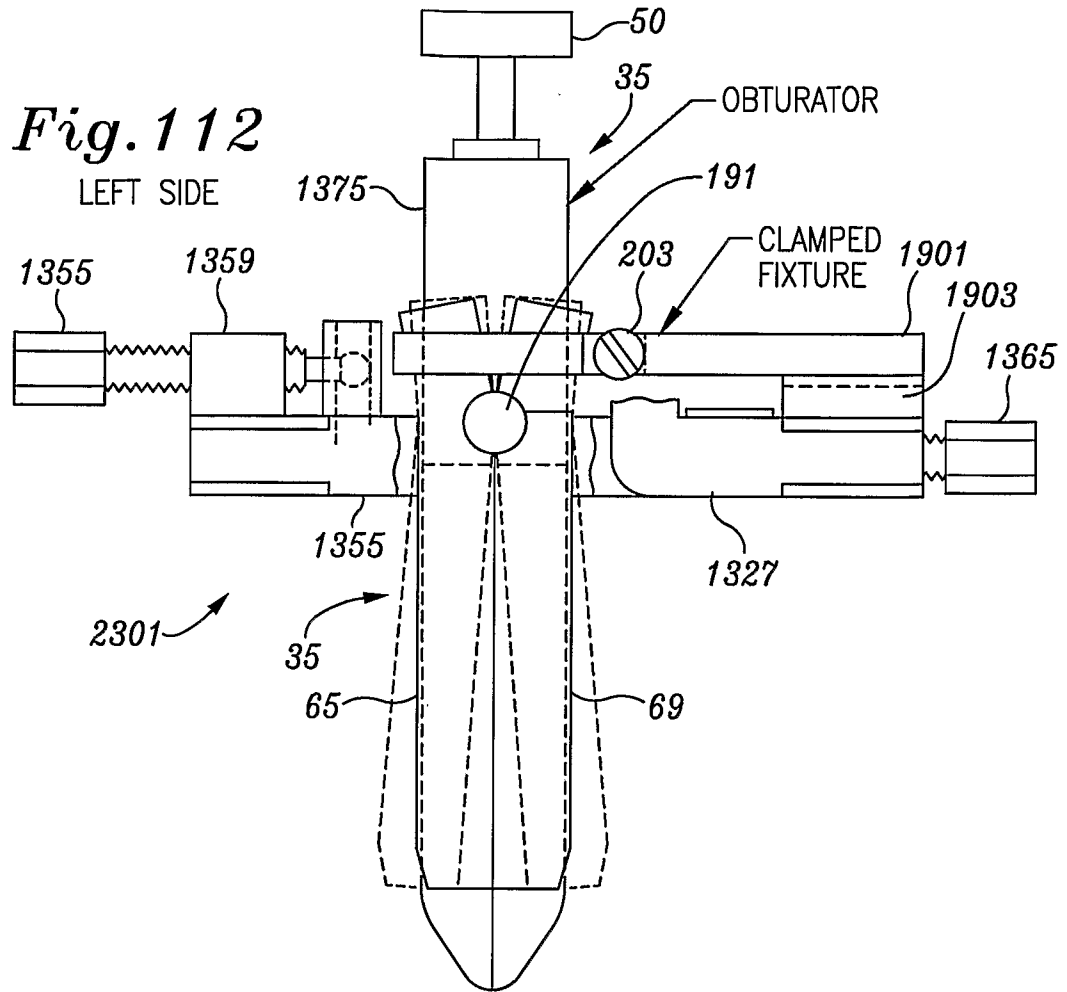


Fig. 113

(PARTIALLY BROKEN VIEW OF CLAMP FIXTURE)

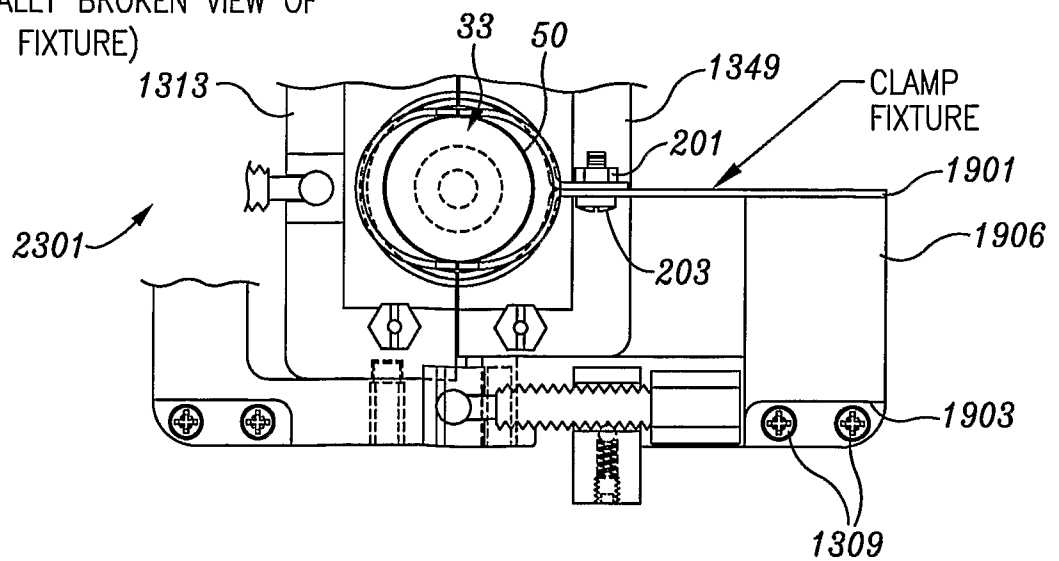


Fig. 119

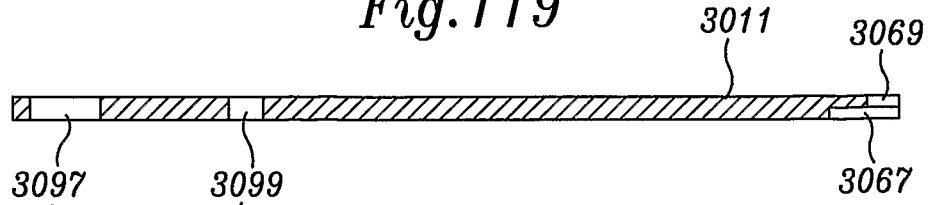


Fig. 117

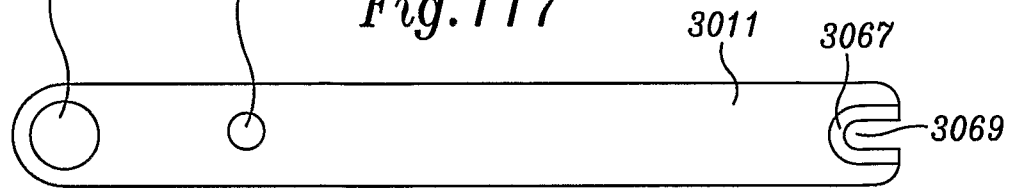


Fig. 115

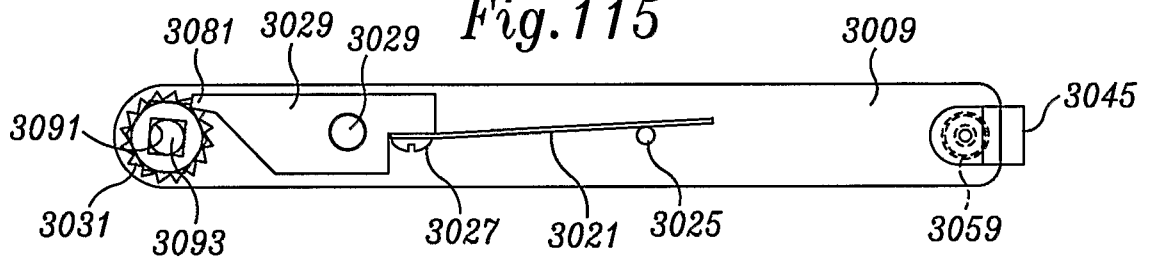


Fig. 114

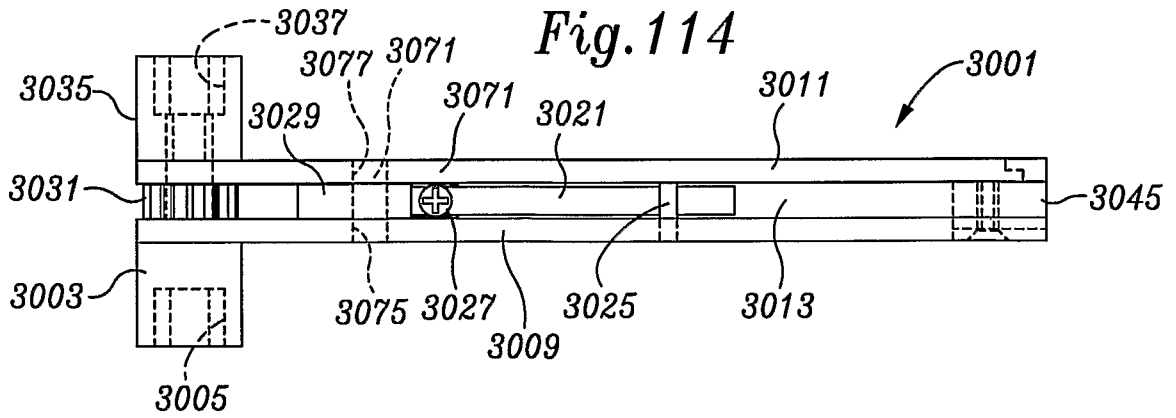


Fig. 118

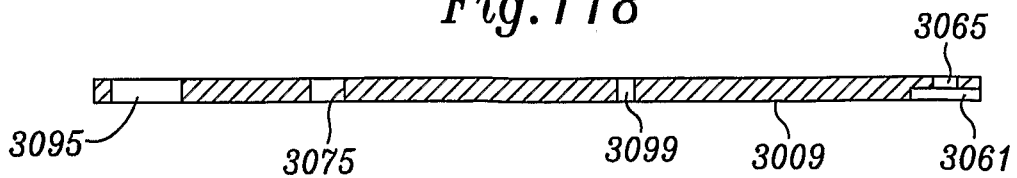


Fig. 116

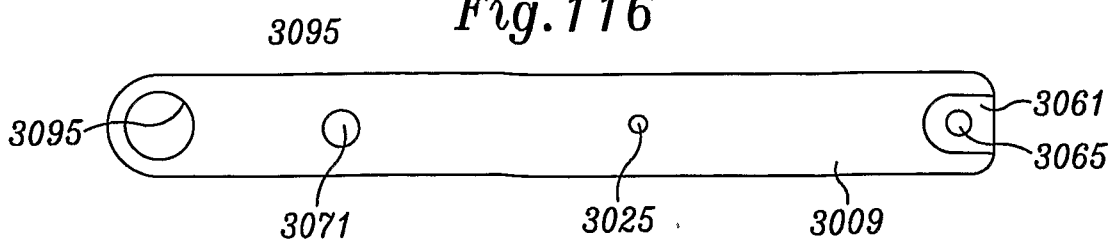


Fig. 125

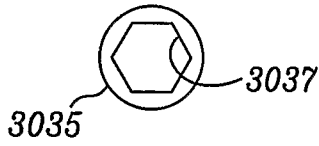


Fig. 124

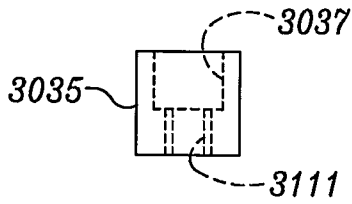


Fig. 126

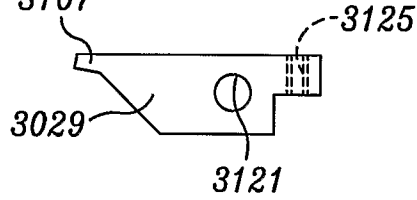


Fig. 123

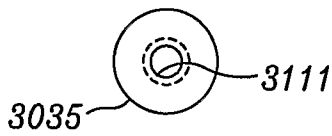


Fig. 127

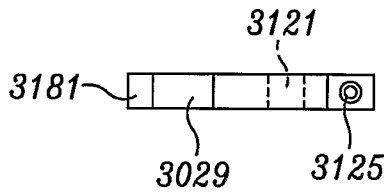


Fig. 122

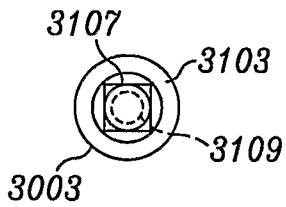


Fig. 128

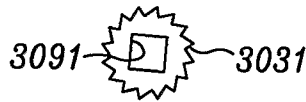


Fig. 129

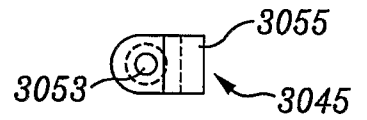


Fig. 121

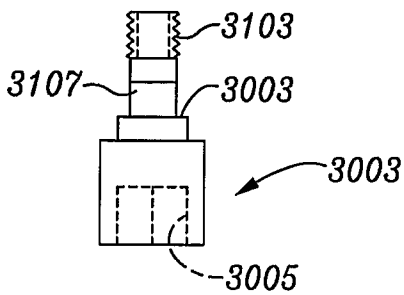


Fig. 120

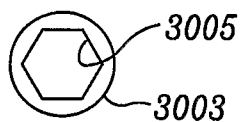


Fig. 130

