

**(12) PATENT
(19) AUSTRALIAN PATENT OFFICE**

**(11) Application No. AU 199871003 B2
(10) Patent No. 742613**

(54) Title
Neocartilage and methods of use

(51)⁷ International Patent Classification(s)
A61F 002/08

(21) Application No: **199871003** (22) Application Date: **1998.04.03**

(87) WIPO No: **WO98/44874**

(30) Priority Data

(31) Number **60/043369** (32) Date **1997.04.04** (33) Country **US**

(43) Publication Date : **1998.10.30**

(43) Publication Journal Date : **1998.12.17**

(44) Accepted Journal Date : **2002.01.10**

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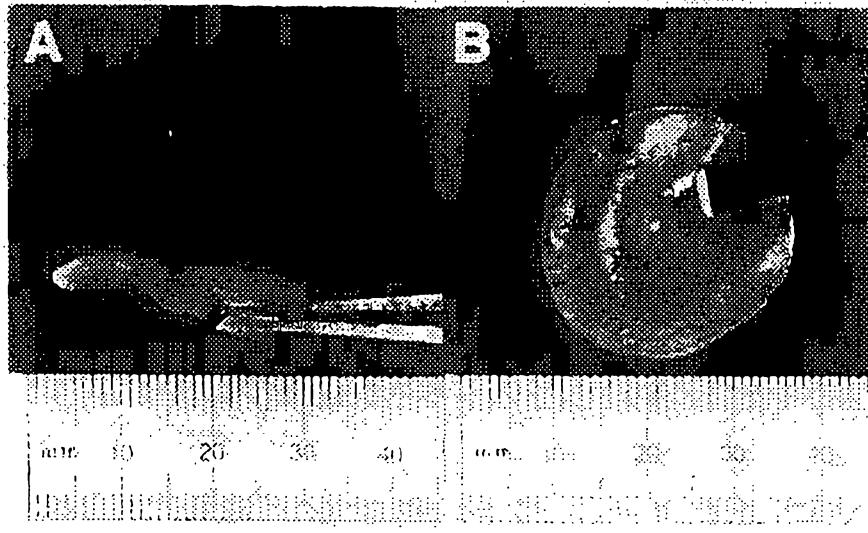
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International Bureau

71003/98

INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶ : A61F 2/08		A1	(11) International Publication Number: WO 98/44874
(21) International Application Number: PCT/US98/06586			(43) International Publication Date: 15 October 1998 (15.10.98)
(22) International Filing Date: 3 April 1998 (03.04.98)			
(30) Priority Data: 60/043,369 4 April 1997 (04.04.97)		US	
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			(Published) <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>
			IP AUSTRALIA 12 MAY 1999

(54) Title: **NEOCARTILAGE AND METHODS OF USE**

(57) Abstract

Disclosed are neocartilage compositions characterized by having multiple layers of cells, said cells being surrounded by a substantially continuous insoluble glycosaminoglycan and collagen-enriched hyaline extra-cellular matrix, and which neocartilage phospholipids are advantageously enriched in anti-inflammatory n-9 fatty acids, particularly 20:3 n-9 eicosatrienoic or Mead acid. Also disclosed are methods of growing neocartilage in substantially serum-free growth media and methods of producing a conditioned growth media containing compounds effective to enhance neocartilage formation. The neocartilage compositions are useful as implants and as replacement tissue for damaged or defective cartilage and as a model system for studying articular cartilage disease and response to natural and synthetic compounds.

NEOCARTILAGE AND METHODS OF USEBACKGROUND OF THE INVENTION

This invention relates generally to novel neocartilage compositions useful as implants and as replacement tissue for damaged or defective cartilage, as model systems for studying articular cartilage disease and articular cartilage response to natural and synthetic compounds and for the isolation of cartilage derived substances useful in the biotechnology industry.

More specifically, the invention concerns neocartilage, particularly human neocartilage, having multiple layers of cells surrounded by a substantially continuous insoluble glycosaminoglycan and collagen-enriched hyaline extracellular matrix, and whose membrane phospholipids are enriched in the anti-inflammatory n-9 fatty acids, particularly 20:3 n-9 eicosatrienoic or Mead acid. Also provided are methods of producing neocartilage *in vitro* by growing chondrocytes in substantially serum-free growth media. The invention further relates to methods for producing conditioned growth media comprising compounds effective to enhance neocartilage formation, and for the isolation of cartilage derived substances.

Unlike most tissues, adult articular cartilage does not self-repair. Normal articular cartilage is hyaline cartilage comprising a distinctive combination of cartilage-specific collagens (types II, VI, IX, and XI) and aggregating proteoglycans (aggrecan) which give it the unique ability to withstand compressive forces.

Chondrocytes are the cartilage-specific cells which give rise to normal articular cartilage tissue growth *in vivo*. Adult chondrocytes, however, have generally lost their potential to reproduce and generate new cartilage *in*

vivo, although they are responsible for maintaining tissue homeostasis.

Attempts to grow human articular cartilage using traditional cell culture methods such as growing 5 chondrocytes on tissue-culture plastic surfaces using serum-containing growth media have proved unsuccessful. Although serum (the non-red blood cell portion of blood, clotted and spun down) is known to be a potent mitogen to chondrocytes, their culture in serum-containing growth 10 media has been reported to result in dedifferentiation of the chondrocyte phenotype.

It is also well known in the art that growing chondrocytes in monolayers on plastic culture vessels for prolonged periods leads to loss of their spherical shape 15 and the acquisition of an elongated fibroblastic morphology. Reginato, et al., *Arthritis & Rheumatism* 37: 1338-1359 (1994). Biochemical changes associated with this morphological change include loss of the articular cartilage phenotype, e.g., loss of rounded cell shape, an 20 arrest of cartilage-specific collagen and proteoglycan synthesis, the initiation of collagen type I and III synthesis, and an increase in small non-aggregating proteoglycan synthesis. Reginato, et al., supra.

Adult human chondrocytes grown directly on tissue-culture plastic in growth media containing serum, attach to 25 the plastic substrate and fail to deposit an insoluble matrix enriched in glycosaminoglycan. Glycosaminoglycan is the proteoglycan component essential to the physiological function of articular cartilage and is the hallmark of 30 hyaline tissue. The extracellular matrix initially produced by methods using serum-containing growth media is not enriched in glycosaminoglycan and resorption of the matrix material occurs as the cell culture ages.

Attempts to overcome chondrocyte dedifferentiation *in* 35 *vitro* have included culturing chondrocytes at high densities and growing them in suspension culture or on

substrata that prevent cellular spreading and attachment to the tissue-culture plastic. Reginato et al. described a method of growing human fetal chondrocytes cultured on polyHEMA-coated plastic dishes in a serum-supplemented DMEM growth media. *Arthritis & Rheumatism* 37: 1338-1359 (1994). This method was successful at maintaining the cartilage-specific phenotype but produced only nodules resembling articular cartilage, not a continuous layer of articular cartilage tissue.

10 Kuettner described in U.S. Pat. No. 4,356,262, a method of producing bovine cartilaginous tissue from which an anti-invasion factor may be recovered. This method provided culturing a monolayer of chondrocytes at high densities in a suspension of serum-containing growth media 15 in a roller bottle. This method produced nodules of tissue having an extracellular matrix, but not a continuous layer of articular cartilage tissue.

Another method that prevents chondrocyte attachment to tissue culture plastic is described in Kandel, U.S. Pat. 20 No. 5,326,357. Kandel described methods of reconstituting bovine cartilage tissue *in vitro* by seeding chondrocytes on a porous tissue culture insert substrate which had been coated with type I collagen to facilitate chondrocyte attachment and growth in a serum-containing growth media. 25 The tissue culture insert is used to separate the chondrocytes from the tissue culture plastic. This method produced a continuous cartilaginous tissue having zones of elongated and spherical chondrocytes which resemble native bovine cartilage.

30 Without a readily available replacement tissue, recent methods of articular cartilage repair have focused on biological resurfacing of cartilage defects with either a prosthetic device or with live chondrocytes. Methods of *in vivo* articular cartilage repair include transplanting 35 chondrocytes as injectable cells or as a composition of cells embedded in a three-dimensional scaffold. These

methods, like *in vitro* neocartilage production, have been less than completely successful. One such repair method is autogenous chondrocyte transplantation. Vacanti et al., WO 90/12603. In this method, normal chondrocytes obtained from the patient are surgically removed, cultured to increase cell number and then injected into the defective site and secured in place with a periosteal flap. Brittberg, M., et al., *N. Eng. J. of Med.*, 331:889-895 (1994). This method requires two separate surgical procedures to complete.

Allograft transplant methods, which require a single surgery, use implants made of donor chondrocytes seeded and grown on a natural or synthetic three dimensional scaffold (Vacanti, et al., U.S. Pat. No. 5,041,138; Gendler, EP 0739631 A2). In these methods, the natural or synthetic three-dimensional scaffold is provided to give the cell culture structure and to mimic the natural extracellular matrix while the cartilage tissue is produced *in vivo*.

It has recently been shown, however, that neither the autogenous nor the allogenic transplant method results in consistent growth of articular cartilage *in vivo*, but rather results in chondrocyte dedifferentiation and formation of fibrocartilage. Because of the reduced aggrecan content of fibrocartilage, it cannot withstand the same biomechanical stresses as articular cartilage. Fibrocartilage degenerates with use, and its formation following joint repair may promote joint dysfunction and permanent disability.

In addition to the clinical need for readily available replacement tissue, healthy articular cartilage is needed for use in model systems for studying articular cartilage disease and to evaluate chondrocyte responses to growth factors, cytokines and pharmaceutical compositions.

Osteoarthritis, the most common form of arthritic disease, affects almost 16 million people in the United States alone. Osteoarthritis is characterized by the

appearance of focal lesions at the cartilage surface. With advancing age and disease progression, these changes are accompanied by a marked reduction in proteoglycan content, extensive destruction of the collagen framework, a marked 5 increase in tissue hydration, and subsequent joint dysfunction.

Osteoarthritis appears to develop within the articular cartilage of weight-bearing joints, particularly joints of the knee, hip, hand, and foot. Under normal physiological 10 conditions, cartilage homeostasis is maintained by the resident chondrocytes. This highly specialized cell functions to synthesize, assemble, and remodel all components of cartilage extracellular matrix, including aggregating proteoglycan as well as collagens type II, VI, 15 IX, and XI. Despite intensive research efforts to ascertain the biological basis of osteoarthritis, its development and progression remain poorly understood.

Recent studies attempting to characterize collagenolytic activity in human osteoarthritis indicate a 20 clear need for a reliable alternative to animal models for elucidating early biological events of disease progression. Most animal tissues do not express the complexity of enzymes that have been implicated in human disease. Thus, 25 animal models are inadequate for evaluating the efficacy of potential disease modifying agents in human osteoarthritis.

A shortage of normal articular cartilage for studying articular cartilage disease and articular cartilage response to natural and synthetic compounds exists because the only source of healthy articular cartilage currently 30 available is from deceased adult donors which may show degenerative changes.

BRIEF SUMMARY OF THE INVENTION

Among the several objects of the invention, therefore, may be noted:

- the provision of novel neocartilage compositions and uses thereof;
- the provision of methods of producing such novel neocartilage compositions and methods of producing conditioned growth media for use therein, and the provision of cartilage specific components useful in tissue engineering.

The neocartilage of the invention is useful, for example, as replacement tissue for damaged or defective cartilage and as a model system for studying articular cartilage disease and response to natural and synthetic compounds. Illustratively, surgical implants, or allografts, of the neocartilage were created *in vitro* and surgically attached to natural cartilage in animal models to repair surgically created defects.

Briefly, therefore, the present invention is directed to neocartilage characterized by one or more of the following attributes: containing membrane phospholipids enriched in Mead acid, containing membrane phospholipids depleted in linoleic or arachidonic acid, being substantially free of endothelial, bone and/or synovial cells, having a S-GAG content of at least about 400 mg/mg of OH-proline, being substantially free of type I, III and X collagen, containing a matrix substantially free of biglycan, being enriched in high molecular weight aggrecan, being produced *in vitro* using serum-free growth medium, being essentially free of non-cartilage material, and being characterized by having multiple layers of cells surrounded by a substantially continuous insoluble glycosaminoglycan and collagen-enriched hyaline extracellular matrix.

The present invention is further directed to methods of growing neocartilage in substantially serum-free growth

media. Initially, chondrocytes are isolated and adhered to a surface using means effective to produce a monolayer cell culture. The cell culture is then grown in a substantially serum-free cell culture to produce the neocartilage of the invention and the neocartilage so produced.

5 The invention is also directed to a biological material containing essentially purified cartilage-specific macromolecules.

10 Also provided is a conditioned growth medium adapted for use in growing cartilage cell cultures which contain heparin-binding growth factors, at least one of which is a cartilage-derived morphogenetic protein (Chang et al., *J. Biol Chem* 269:28227-28234).

15 In a further aspect of the invention, a set of implant materials are provided. These materials include a reparative amount of Mead acid enriched neocartilage or neocartilage produced as described above. Also included are means for implanting and adhering the neocartilage in a target tissue locus.

20 In yet other aspects of the invention, methods of producing a conditioned growth media comprising compounds effective to enhance neocartilage formation and such conditioned growth media are provided, and methods of producing cartilage derived compounds and such cartilage-derived compounds, using serum-free growth media, are also provided.

25 In an additional aspect of the invention, a method of screening a pharmaceutical for its capacity to modulate arthritic disease is provided. In this method, the neocartilage as described herein is co-cultured with the pharmaceutical in an amount and under conditions effective for determining whether characteristic indications of arthritic modulation are observed in the neocartilage.

30 Other objects and features will be in part apparent and in part pointed out hereinafter.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1, in two parts, FIGS.1A and 1B, shows gross morphology of human neocartilage produced *in vitro*. Fetal chondrocytes grown under serum-free conditions to day 120 produce hyaline tissue that is roughly 1.5-2 mm thick. Wet weights of 300-400 mg were obtained from material grown in 12 well dishes. FIGS.1A and 1B, respectively, represent lateral and birds-eye views of human neocartilage at day 90 of culture. The structural characteristics of this hyaline cartilage mimics that of native articular cartilage.

FIG. 2 is a graphical representation which shows growth curves for fetal chondrocytes grown in the presence (solid line) and absence (dashed line) of serum. DNA content was measured over a 60-day time course using Hoechst 33528 fluorescent dye, following papain digestion. Herring sperm DNA was used as standard. Chondrocytes grown under the specified serum-free conditions go through the same number of doublings as those cells grown in the presence of serum.

FIG. 3, in two parts, FIGS.3A and 3B, is a graphical representation which shows that serum deprivation promotes neocartilage formation *in vitro*: Glycosaminoglycan and collagen deposition by fetal human chondrocytes. Chondrocytes were isolated from the upper region of the proximal tibia and distal femur of human fetal knees (18-21 wks gestation) by sequential enzymatic digestion. Cell suspensions were then filtered, counted, and seeded at high density (24 well clusters) in media containing 10% serum to allow adherence. Upon reaching confluence (day 7), the cultures were subdivided into two groups such that half of the dishes remained serum-free (dashed line), while the remaining dishes were maintained in serum-containing media (solid line). Growth media were supplemented with 50 µg/ml ascorbate at every media change, usually every 72 h. Sulfated glycosaminoglycan

(S-GAG) (**FIG.3A**), and hydroxyproline (OH-proline) (**FIG.3B**), content of the newly synthesized, insoluble hyaline matrix were measured as described hereinbelow. Chondrocytes grown under serum-free conditions produced 5 at least 10-fold greater amounts of proteoglycan (sulfated glycosaminoglycan) and more than 2-fold greater levels of collagen (hydroxyproline) as compared to parallel cultures that were maintained in 10% FBS.

FIG. 4, in two parts, **FIGS.4A and 4B** shows the 10 morphologic appearance of human neocartilage (day 56) following serum repletion (10% FBS). Day 28 neocartilage was treated with 10% FBS until termination on day 56 (**FIG.4B**), at which point neocartilages were fixed and 15 stained with safranin-O to visualize aggrecan. **FIG.4A**, day 56 control neocartilage (serum-free). Notice the marked decrease in metachromatic staining which occurred in response to repletion with 10% FBS (**FIG.4B**). Also notice the flattened and elongated phenotype of chondrocytes present at the surface of the neocartilage. 20 These changes suggest that in the absence of mechanical stimulation, serum promotes autolytic resorption of hyaline cartilage matrix, the mechanism of which requires further study.

FIG. 5, in six parts, **FIGS.5A - 5F** shows the 25 morphologic appearance of native and neocartilage matrix following formalin fixation and paraffin embedding. Tissue sections were cut and stained with either safranin-O (**FIGS.5A, 5C and 5E**) or pentachrome (**FIGS.5B, 30 5D, and 5F**) to visualize specific extracellular matrix components.

Safranin-O stains red and identifies S-GAG, whereas pentachrome stains yellow for collagen, green for proteoglycan, and black for elastin. Because the tissues are enriched in collagen and proteoglycan, an aqua blue 35 color is achieved upon pentachrome staining.

FIGS.5A and 5B show longitudinal sections of fetal proximal tibia used to create the neocartilage grafts in **FIGS.5C - 5F**.

5 **FIGS.5C and 5D** represent neocartilage grown under serum-free conditions and harvested at day 90.

FIGS.5E and 5F demonstrate the inhibitory effect of serum on neocartilage formation (day 0-30). (10% FBS).

Serum supplementation caused the cell layers to ball up and slough away from the tissue culture surface after 10 day 30. Note that **FIGS.5C and 5D** show only a small fraction of the full thickness of day 90 neocartilage. Chondrocytes are seen localized to individual lacunae, forming hyaline tissue that is virtually indistinguishable in appearance from the native starting 15 material and which spans 15-20 cell layers deep.

Magnification x 200 for **FIGS.5A, 5B, 5E and 5F**, and x 400 for **FIGS.5C and 5D**.

20 **FIG. 6**, in six parts, **FIGS.6A - 6F** shows the ultrastructural characterization of neocartilage matrix by transmission electron microscopy (TEM). Representative cultures from **FIG. 5** were fixed with glutaraldehyde, post fixed with osmium-tetroxide, and stained en-bloc with tannic acid and uranyl acetate. Ultra-thin sections were counter-stained routinely with uranyl acetate and lead 25 citrate. High power magnification x 61,900 (B,D,F) of the ECM of native (**FIGS.6A and 6B**) and neocartilage tissue grown in either the presence (**FIGS.6E and 6F**), or absence (**FIGS.6C and 6D**) of 10% FBS.

30 Note that **FIG.6E** represents the entire thickness of the culture material and that these chondrocytes display cell/cell contact. Type II collagen (20 nm diameter fibrils) comprised the dominant structural protein in each of these tissues, confirming that the engineered tissue is hyaline in nature. Low power magnification x 35 3,365 (A,C,E). A lack of matrix proteoglycan probably

contributes to stacking of the collagen fibrils observed in FIG.6F.

FIG. 7 shows SDS-PAGE and Western analysis of matrix associated collagen obtained by limited pepsinization and 5 neutral salt precipitation.

- S1 and S2 are duplicate samples of neocartilage tissue (day 90), while FC and Sk represent native fetal cartilage and skin, respectively.
- Antibodies to collagen types-II, IX and I were obtained from Oncogene Sciences.

10 The analysis shows the presence of type II collagen and the absence of type I collagen. Only the positive control (fetal skin) recognized monoclonal antibody directed to collagen type I.

15 FIG. 8, in two parts, FIGS.8A and 8B, shows cytokine-induced resorption of fetal articular cartilage. It is a demonstration of the relative appearance of treated and untreated neocartilage cultures showing that neocartilage exposed to cytokine is markedly reduced in 20 size and lifts away from the plastic surface.

- Tissue was propagated as described above (day 28) and stimulated with increasing concentrations of the indicated cytokine or growth factor (FIG.8B) for an additional 36 days.
- Cytokines were added to fresh ascorbate containing media every 48 hours.
- Spent media was collected and frozen at each feeding for analysis of S-GAG, hydroxyproline content, and matrix metalloproteinase (MMP) 30 synthesis.
- Likewise, remnant neocartilage was frozen for chemical analysis of ECM components.

Note that in each case, the IL-1 and TNF-treated samples retracted considerably upon removal from the plastic surface (FIG. 8A), implying that increased synthesis and activation of the MMPs reduced the structural integrity 5 of the tissue.

FIG. 9, in four parts, FIGS. 9A - 9D, shows a comparison of the extracellular matrix of control (FIGS. 9A and 9B) and activated (FIGS. 9C and 9D) neocartilage following stimulation with interleukin-1. It is seen 10 that chronic IL-1 stimulation alters cartilage staining for proteoglycan and collagen.

- Day 60 neocartilages were treated with 1 ng/ml rhIL-1 β for 30 days. Fresh media and cytokine were added every 48 hours.
- 15 - Neocartilages were harvested (day 90) and stained with safranin-O and pentachrome as before. Staining intensity is markedly reduced in stimulated (FIGS. 9C, 9D) versus untreated controls (FIGS. 9A, 9B).
- 20 - Chondrocyte activation with IL-1 caused a significant reduction in the thickness of the synthesized matrix. Altered pentachrome staining following IL-1 stimulation suggests that MMP-mediated cleavage of collagen directly affects the binding characteristics of pentachrome dye to collagen. Magnification x100.
- 25

FIG. 10, in two parts, FIGS. 10A and 10B, represent SDS-substrate gel (zymogram) analysis of cytokine-mediated production of matrix metalloproteinases (MMPs) 30 in fetal articular chondrocytes (neocartilage disks). Negative staining indicates the molecular weight (MW) in kDa of the active proteases.

- Spent media were collected 72 h post stimulation with the indicated cytokine (5 ng/ml) and concentrated 16-fold by dialysis/lyophilization.
- 5 - Unreduced samples were separated on 10% SDS substrate gels containing either gelatin (**FIG.10A**) or casein (**FIG.10B**) 0.1%.
- MMPs were renatured following SDS removal by extensive washing in 2.5% Triton X-100 and 10 lytic bands visualized via negative staining with Coomassie blue, following incubation in a calcium and zinc containing buffer for 4 hr at 37°C.
- 15 - Latent enzyme activity is shown in lanes 1-4, while the corresponding active enzymes were prepared by preincubation with 1 mM 4-aminophenyl mercuric acetate (APMA lanes 5-8).

20 **FIG. 11**, in two parts, **FIG.11A** and **FIG.11B**, is an immunoblot demonstrating cytokine-induced production of collagenase-1 (**FIG.11A**) and collagenase-3 (**FIG.11B**) in culture media.

- Cell layers were stimulated chronically with 5 ng/ml rhIL- β and the spent media collected every 72 h.
- 25 - Twenty μ l fractions were reduced and immunoblotted with monospecific polyclonal antisera to collagenase-1 (**FIG.11A**) and collagenase-3 (**FIG.11B**).
- Positive controls (purified recombinant protein) for each blot are shown in lane 1 and ranged in size from 50-54 kDa.
- 30 - Media control, Lane 2; unstimulated control, lanes 3-4; 3-day stimulation, lane 5; 6-day stimulation, lane 6.

FIG. 12, in four parts, FIGS.12A, 12B, 12C, and 12D, shows a surgical model for articular repair. Arthrotomy was performed by a medial parapatellar incision and lateral patella dislocation. A full-thickness cartilage defect, measuring 3 mm from proximal to distal traversing 5 mm from the medial edge of the medial femoral condyle, was created using a No. 15 scalpel. The defect was curetted down to, while not violating, the subchondral bony plate. The medial side of the neocartilage graft was sutured to the periosteum of the medial femur, while the lateral aspect of the graft was sutured to host cartilage at the lateral edge of the defect using 7-0 Proline sutures. After applying tissue transglutaminase (Sigma Chemical Co.) under the graft via syringe (Jurgensen et al., *J Bone Joint Surg*, 79-A:185-193, 1997), the graft-defect interface was stabilized for five minutes via finger pressure. The patella was then reduced, and the arthrotomy closed in layers with interrupted 5-0 Ethibond suture. The skin incision was closed with interrupted subcuticular 5-0 Proline sutures. Medial and anterior aspects of the operated knee are depicted in FIGS.12A, 12C, and in FIGS. 12B, 12D, respectively.

FIG. 13, in two parts, FIGS.13A and 13B show the gross appearance of rabbit knees at harvest following surgical implantation of rabbit neocartilage. Three by 5 mm (3 x 5) experimental defects were created in the medial femoral condyles of 30 wk New Zealand White rabbits. Gross inspection six weeks post-operatively revealed that the neocartilage allograft was in place (FIG.13B), and has taken on the appearance of the surrounding native cartilage. The unfilled defect of the contralateral knee remained empty (FIG.13A).

FIG. 14, in two parts, FIG.14A and FIG.14B, shows the results of two separate one-way mixed leukocyte assays used to measure alloreactivity via lymphocyte

proliferation. The experiment in **FIG. 14B** was set up to investigate alloreactivity of neocartilage, following enzymatic dissociation with collagenase and hyaluronidase. Legend: A = chondrocytes isolated from day 40 neocartilage (fetal donor); B = chondrocytes isolated from day 30 culture (20 year male donor); C = chondrocytes isolated from day 30 culture (27 year male); D = chondrocytes isolated from day 30 culture (36 year female).

10 - In **FIG.14A**, 1×10^5 irradiated peripheral blood leukocytes (PBL, American Red Cross, St. Louis, Missouri) from two unrelated donors were mixed with non-irradiated PBL from either the first (auto) or second donor (allo). Tritiated

15 thymidine was added on day 6. Cultures were harvested and the amount of radiolabel incorporated into newly synthesized DNA counted.

20 - In **FIG.14B**, 1×10^5 irradiated chondrocytes from four different donors of 20-36 yrs age were incubated with 1×10^5 non-irradiated PBL and their proliferation measured on day 7. Chondrocytes failed to stimulate proliferation of allogeneic PBL obtained from donor 2.

25 Positive (allo) and negative (auto) controls were run on the same plate and are included for comparison. Legend: PBL1=peripheral blood leukocytes from unrelated donor 1; PBL2=peripheral blood leukocytes from donor 2.

30 **FIG. 15** shows the co-stimulatory function of human neocartilage chondrocytes. 1×10^5 T-cells, semi-purified from donor 2 (**FIG.14A**) using affinity columns from R & D Systems, were incubated with irradiated chondrocytes used in **FIG.14**. Incubations were carried out at 37°C for

three days. Again, chondrocytes failed to stimulate a proliferative response above background.

FIG. 16 is a bar chart which shows that overlaying neocartilage with secondary passage of chondrocytes increases allograft thickness and rigidity. Day 10 human neocartilage (12 well dishes) was overlayed with 5×10^5 chondrocytes obtained via secondary passage. These cultures were harvested at day 28 and compared to control cultures that were initially seeded with 1×10^6 cells/well.

FIG. 17, in two parts, FIGS. 17A and 17B, is a characterization of neocartilage proteoglycans on 1.2% agarose gels. Human neocartilage (day 35) was labeled for 72 hr with carrier-free sodium sulfate ($10 \mu\text{Ci}/\text{ml}$). Matrix proteoglycans were then guanidine extracted, ethanol precipitated, and extensively dialyzed prior to fractionation on 1.2% agarose gels. FIG. 17A, toluidine blue stained proteoglycan. FIG. 17B, autoradiograph showing localization of incorporated label in six replicates of neocartilage. Trace amounts of decorin were identified in six replicates of neocartilage, whereas biglycan, present in the 12- and 43-year subjects, was not synthesized. Lanes: 1 (chondroitin-4-sulfate standard); 2 (12-yr female); 3 (43-yr male); 4-9 (replicates of human neocartilage). Note that native decorin can only be viewed in the neocartilage following metabolic labeling.

FIG. 18, in two parts, FIGS. 18A and 18B shows the effect of heparin on neocartilage formation. Day 10 neocartilage was treated with increasing amounts of heparin for 18 days. Fresh media, containing heparin and ascorbate were added every 72-96 hrs. Media were collected and frozen for future analysis. Cultures were harvested on day 28 and the S-GAG content (FIG. 18A) and OH-proline content (FIG. 18B) of the resultant neocartilage assayed as described hereinbelow.

FIG. 19 shows cartilage-derived morphogenetic proteins (CDMP's) in human neocartilage matrix. Neocartilage formed by 90-day cultures of chondrocytes from donors of various ages were extracted in a 1.2 M 5 guanidine-HCl buffer and passed over a heparin affinity column. Proteins were eluted with 1 M NaCl and concentrated using a Centricon filter with a 10K cutoff. The proteins were electrophoresed on a 12% SDS gel under reducing conditions, and transferred to Immobilon 10 (Millipore) membranes. Immunoblots were probed with anti-CDMP antibody (N442) provided by the NIH. The secondary antibody was detected using chemiluminescence. Lanes: 1 (fetal; 2 (1-day neonate); 3 (8-month infant); 4 (12-yr adolescent); 5 (48-year adult). 15 Immunoreactivity was detected in 56 Kd pre-forms, 34 Kd dimers and 14-17 Kd mature proteins.

FIG. 20, in six parts, FIGS. 20A - 20F, shows the fatty acid composition of human neocartilage phospholipids versus time. Chondrocytes were grown in either 20 the presence (open circles) or absence (filled circles) of 10% serum as described herein and the fatty acid composition of the membrane phospholipids isolated via silicic acid chromatography determined via capillary gas chromatography. The upper panels (FIGS. 20A, 20B and 20C), correspond to the n-6 polyunsaturated fatty acid precursors of eicosanoid synthesis, while the lower panels (FIGS. 20D, 20E and 20F) designate the n-9 fatty acids which are abundant in rapidly growing hyaline 25 cartilage. Notice that Mead acid (20:3 n-9 eicosatrienoic acid) accumulates under serum-free conditions to a level that was two-fold greater than that identified in the native tissue at time zero. Additionally, serum supplementation caused a three-fold 30 accumulation in arachidonate (20:4 n-6). The Mead-to- 35 arachidonate ratio of serum vs. serum-free cultures mirrored that identified in adult and fetal tissue,

respectively (Adkisson et al., 1991, supra). Samples were run in duplicate.

FIG. 21 is a mass chromatogram showing the dominant polyunsaturated fatty acid identified in neocartilage phospholipids (i.e. 20:3 n-9 eicosatrienoic acid) at day 5 28 of culture. The fragmentation pattern matches that of authentic 20:3 n-9 eicosatrienoic or Mead Acid.

FIG. 22, in two parts, FIGS. 22A and 22B, shows the morphologic appearance of neocartilage/demineralized bone 10 (Lambone) composites following pentachrome staining. Magnification: 22A, 100x; 22B, 200x.

DETAILED DESCRIPTION OF THE INVENTION

In accordance with the present invention, applicant has produced neocartilage tissue which has a morphological 15 appearance largely indistinguishable from healthy native articular cartilage. The cartilage produced is strong, yet malleable. It is readily removable from culture vessels and can be grown with or without the aid of a three-dimensional scaffold. Moreover, this novel cartilage has 20 a membrane phospholipid fatty acid profile which is conducive to resistance to transplant rejection and inflammation. This newly developed biological material also serves as a ready resource for obtaining purified compositions important for applications in biotechnology, 25 including cartilage-specific macromolecules such as high molecular weight aggrecan and collagen types II, VI, IX and XI.

The biological material hereby provided comprises neocartilage having multiple layers of cells surrounded by 30 a substantially continuous insoluble glycosaminoglycan and collagen enriched hyaline extracellular matrix. Furthermore, the membrane phospholipids of the neocartilage are unexpectedly and advantageously enriched in 20:3 n-9 eicosatriene (Mead) fatty acids and depleted in 35 linoleic and arachidonic fatty acids. The Mead acid

content is preferably at least about 2% and most preferably, between about 2.5% and 10% of the total fatty acid content. The linoleic acid and arachidonic acid content is preferably less than about 0.5% and most 5 preferably at least about 0.2% of the total fatty acid content of the membrane phospholipids. This neocartilage is further characterized by its high S-GAG and hydroxyproline content, enrichment in high molecular weight aggrecan, and the relative absence of endothelial, bone and synovial 10 cells, as well as being substantially free of biglycan. Preferably, the neocartilage has a S-GAG content of at least about 400 mg/mg of OH-proline, and more preferably, from about 500 mg to about 2500 mg/mg of OH-proline. Preferably, the high molecular weight aggrecan contains at 15 least about 80%, and more preferably, it contains about 90%, of the total cartilage proteoglycan content. The chondrocytes of the neocartilage of the present invention are substantially spherical throughout the composition and maintain their articular cartilage phenotype. The 20 neocartilage composition of the present invention is a substantially continuous layer of tissue at least two cell layers thick. After 14 days of growth, the neocartilage had grown to between 10 and 15 cell layers thick. The neocartilage can be grown for at least 120 days to a 25 thickness of at least 2mm and to a weight of between 300 and 400 mg when 3.8 cm² dishes are used (15-20 cell layers thick).

The neocartilage can be grown to substantially greater thicknesses when grown under conditions that mimic the 30 biomechanical forces to which articular cartilage is naturally subjected *in vivo* such as in a compression chamber. It has been found that after 30 days of growth, and as described herein, the glycosaminoglycan content of the neocartilage is approximately 600-1,500 mg S-GAG/mg OH-proline. This is 10 times greater than that of 35 chondrocytes grown in the presence of 10% serum.

5 The neocartilage may comprise avian or mammalian chondrocytes, preferably human chondrocytes. Additionally, mammalian chondrocytes may be derived from transgenic animals which have been genetically engineered to prevent
10 immune-mediated xenograft rejection (Sandrin, MS et al., *Nature Med* 1:1261-1267, 1995; Sandrin, MS et al., *Xenotransplantation* 3:134-140, 1996; and Osman, N et al., *Proc Nat Acad Sci* 94:14677-14682, 1997). Thus, the neocartilage may be mammalian neocartilage, including human and porcine, or avian neocartilage.

15 The use of organs/tissues from animal donors (xenotransplantation) is a potential solution to the chronic shortage of allogeneic organs. Porcine tissues are thought to be most suitable for human use due to similarities in size, anatomy and organ physiology between pigs and humans. Recent insights into the mechanisms underlying vascular rejection, endothelial cell activation, and cellular responses to xenogeneic tissue have led to the development of novel strategies designed to inhibit immune-
20 mediated xenograft rejection (Dorling, A., *Expert Opinion on Therapeutic Patents*, 7:1307-1319, 1997).

25 The neocartilage of the present invention does not require the inclusion of biosynthetic polymer scaffolds in the composition. However, such scaffolds can also be used, if desired. In one alternative embodiment, neocartilage can be grown on demineralized bone allograft forming a composite which is particularly amenable to surgical implementation.

30 Because the neocartilage of the present invention can be produced free of non-cartilage material, its use as an implant or as replacement tissue provides enhanced biocompatibility. For example scaffold-less neocartilage readily integrates into the surrounding tissue whereas cartilage constructs containing artificial polymer
35 scaffolds are likely to take longer to integrate because the cells must first break down the artificial scaffolds.

In another aspect of the invention, the neocartilage can be used as a replacement tissue for the repair of damaged or defective articular cartilage.

- The replacement tissue can be mammalian or 5 avian replacement tissue, most preferably human replacement tissue. Furthermore, mammalian replacement tissue can be produced using chondrocytes from transgenic animals which have been genetically engineered to prevent immune-mediated xenograft rejection.
- The replacement tissue can be implanted using 10 procedures well known in the art, such as using traditional surgical means or by implanting orthoscopically.
- Surgical implants comprising neocartilage can 15 be surgically implanted and attached to natural cartilage *in vivo* by sutures or a combination of sutures and biocompatible biological glues, such as tissue trans-glutaminase (Jurgensen et al., *J. Bone J. Surg.* 79A:185-193.)
- The neocartilage replacement tissue can also be attached to natural cartilage *in vivo* by 20 sutureless attachment such as chemical tissue welding.
- The neocartilage can be grown to various size 25 specifications to facilitate implantation.

Another embodiment of the invention provides using the neocartilage as a model for studying articular cartilage disease and articular cartilage response to natural and 30 synthetic compounds *in vitro*. Natural and synthetic compounds of interest such as enzymes, cytokines, growth factors, anti-invasion factors, dedifferentiation factors and pharmacologic agents are generally known in the art.

In particular, the neocartilage may be used in the testing of pharmacologic agents useful in the treatment of diseases of the joint, for example, osteoarthritis and joint inflammation. Arthritis is marked by an increase in 5 the synthesis and release of a variety of cartilage-derived metalloproteinases and mediators of inflammation. Because these enzymes are directly responsible for tissue destruction in arthritis, the matrix metalloproteinases (MMPs) offer excellent drug targets for the development of 10 novel disease-modifying agents. In this aspect, pharmaceuticals are screened for their capacity to modulate arthritic disease. The neocartilage is co-cultured with a candidate pharmaceutical and observed to determine whether characteristics indicative of arthritic modulation are 15 observed. The amounts and conditions employed are largely dependent on the particular pharmaceutical tested and employ methods well known in the art.

In yet another embodiment of the invention, applicant has discovered a novel method for producing neocartilage 20 compositions *in vitro* from chondrocytes. The method of this embodiment comprises:

- isolating chondrocytes;
- adhering the chondrocyte cells to a surface in a manner effective to produce a cell culture; this 25 may be accomplished by growing the chondrocytes in a growth medium containing an amount of serum effective to allow adherence of the chondrocytes to an appropriate culture vessel;
- replacing the growth media containing an amount 30 of serum with a substantially serum-free growth media to produce a substantially serum-free cell culture; and
- growing the substantially serum-free cell culture 35 to produce neocartilage and neocartilage-derived factors.

In a preferred method, chondrocytes isolated from immature donors such as fetal, neonatal infant, or pre-adolescent chondrocytes are isolated and grown in a substantially serum-free growth media to produce 5 neocartilage.

The chondrocytes used in this method can be avian or mammalian, preferably human chondrocytes. Further, in contrast to other methods of producing neocartilage known in the art, such as seeding cells on three dimensional scaffold material or on material that prevents cellular spreading, further exogenous material is not required to produce three dimensional neocartilage. Unlike methods known in the art, the method of the present invention provides for seeding chondrocytes in direct contact with an 10 appropriate tissue-culture vessel, most preferably uncoated 15 tissue-culture plastic. Although scaffold material is unnecessary, it can be used.

In a preferred embodiment of the invention, a cell culture is produced by isolating immature chondrocytes, 20 e.g., fetal, neonatal, and pre-adolescent chondrocytes from donor articular cartilage.

- Chondrocytes may be isolated by methods known in the art such as by sequential enzyme digestion techniques.
- The isolated chondrocytes may then be seeded directly on a tissue culture vessel in a basal media comprising an effective amount of serum such as Dulbecco's modified Eagle's medium (DMEM) to allow adherence of the chondrocytes directly 25 to the culture vessel and to promote mitogenesis.
- The effective amount of serum added is between 2 and 15% fetal bovine serum, preferably 10%.
- The culture medium may also comprise ascorbate, exogenous autocrine growth factors or conditioned 30 growth media as described below.

- The cell culture may be grown under suitable culture conditions known in the art such as growing the cell culture at 37 degrees C in a humidified atmosphere with the addition of 2-10% CO₂, preferably 5%.
- The growth media containing serum is replaced with growth medium containing half as much serum, preferably 5% of the total growth medium on between day 1 and day 10, preferably on day 7.
- On between day 5 and day 14, preferably day 10, the serum containing growth medium is replaced with substantially serum-free growth media to produce a substantially serum-free cell culture.

15 The preferred substantially serum-free growth media is HL-1, a serum-free media containing insulin-transferrin-selenium-complex as its only source of protein. HL-1 is a registered trademark of Hycor Biomedical, Inc., and also is available from BioWhittaker, Walkersville, Maryland. Other 20 suitable serum-free growth media will be readily apparent to those skilled in the art.

25 The substantially serum-free growth media is preferably partially changed periodically throughout the growth period. Following 10 more days in the substantially serum-free medium, the neocartilage of the invention is between 10 and 15 cell layers thick and can be removed from the cell culture with forceps as a rigid disk of neocartilage.

30 The neocartilage produced by the substantially serum-free cell culture can be grown for at least 300 days. Even after 120 days in culture, the chondrocytes of the neocartilage do not dedifferentiate and fail to synthesize collagen types I, III, and X. The method of the present invention can produce neocartilage of various sizes by 35 using various sized culture vessels.

In yet another aspect of the invention, a method for producing growth media is provided. The method comprises:

- isolating fetal chondrocytes;
- producing a cell culture by growing isolated chondrocytes in a growth media containing an amount of serum effective to allow adherence of the chondrocytes to an appropriate culture vessel;
- replacing the growth media containing an amount of serum with a substantially serum-free growth media after a beginning time interval to produce substantially serum-free cell culture;
- growing the substantially serum-free cell culture to produce conditioned growth media; and
- extracting or concentrating the conditioned growth media from the substantially serum-free cell culture.

The conditioned growth media produced by the method of the present invention can be extracted by means such as heparin affinity chromatography. It may also be concentrated via dialysis and lyophilization. The conditioned growth media thus produced is reserved for future use. The conditioned growth media obtained by this process comprises compounds effective to enhance neocartilage formation such as autocrine factors, dedifferentiation factors, and anti-invasion factors. At least two of these autocrine factors have been identified by applicant as cartilage-derived morphogenetic protein -1 and -2.

When the conditioned growth media is added to the substantially serum free media to between about 5% and 30%, preferably at least about 20% of the total media, it increases the proliferation of neonatal and infant chondrocytes and subsequent deposition of the substantially

continuous insoluble glycosaminoglycan and collagen enriched hyaline extracellular matrix.

In order to illustrate the invention in further detail, the following specific laboratory examples were 5 carried out. Although specific examples are thus illustrated herein, it will be appreciated that the invention is not limited to these specific examples or the details therein.

The sources of various materials used in the specific 10 laboratory examples are as follows:

Materials - Dulbecco's modified Eagle's medium (DMEM) with added L-glutamine, sodium pyruvate, and glucose (4.5 g/liter), fetal bovine serum (FBS) and antibiotic (100x) (penicillin G, sodium (10,000 units) and streptomycin 15 sulfate (25 mg/ml of normal saline) were obtained from Life Technologies, Inc. (Grand Island, NY).

Pronase-E (Type XIV, from *Streptomyces griseus*), hyaluronidase (type III), N-tris[hydroxymethyl]methyl-2-aminoethanesulfonic acid (TES), and MILLEX-GS syringe 20 sterilization filters were obtained from Sigma Chemical Company (St. Louis, MO).

Collagenase (CLS II) was purchased from Worthington Biochemicals (Freehold, NJ). Tissue-culture dishes (12 and 24 well cluster) and bottle top sterilization filter units 25 (type CA) were obtained from Costar Corporation (Cambridge, MA).

Bovine serum albumin (fraction V, fatty acid-free) was from Calbiochem (San Diego, CA). HL-1 growth media, was obtained from Hycor Biomedical (distributed currently by 30 BioWhittaker).

EXAMPLE 1

Preparation and Culture of Immature and Adult Human Chondrocytes - Chondrocytes were isolated within 8-24 hours of death from the upper region of the tibial plateau and 35 femoral condyle of intact fetal bones (18-21 weeks

gestation, Advanced Bioscience Resources, Inc., Alameda, CA). Hyaline cartilage from infant knees (\leq 8 months) was removed from the metaphysis of both the proximal tibia and distal femur using rib cutters and transferred to sterile 5 serum-free DMEM, containing antibiotics (2x) and 1% bovine serum albumin, for chondrocyte isolation as described below. Additional samples of more mature cartilage (12-58 years) were processed similarly. All of these cartilage tissues were provided by Mid-America Transplant Association 10 (St. Louis, MO). All tissues were transported on wet ice prior to use.

Skin from fetal limbs was removed and stored at -20°C for preparation of collagen standards (i.e., types I and III) via limited pepsinization. Skeletal muscle and other 15 connective tissue were dissected under aseptic conditions to expose the articulating surface of the tibia and femoral condyle. The cruciate ligaments, menisci, and synovial capsule were removed.

Articular cartilage was separated from its underlying 20 epiphysis (i.e., more vascularized region), transferred to the cold synthetic cartilage lymph (SCL) described by Majeska and Wuthier, *Biochim Biophys Acta*, 391:51-60 (1975), and washed extensively (4x) to remove contaminating 25 synovial fluid. Any remaining connective tissue was removed from the cartilage by incubation with 1x trypsin-EDTA (Sigma Chemical Co.) for 30 minutes at 37°C. The enzyme solution was replenished with fresh serum-free DMEM and residual trypsin removed by four additional washes using a vortex mixer.

30 At this stage of preparation, the cartilage was glistening white in color and showed no evidence of fibrous tissue contamination. Cartilage was then diced into 1 mm cubes, washed and transferred to 50 ml sterile conical tubes (approximately 2 g tissue/tube) containing 7 ml of 35 pronase-E solution (2 mg/ml Sigma Type XIV from *S. griseus*) in HL-1 for 30 minutes digestion at 37°C in an

environmental incubation shaker set at 200 rpm (New Brunswick Scientific). The enzyme solution was removed and 4 ml of HL-1, containing 1 mg/ml BSA, antibiotics and ascorbate (50 μ g/ml) was added. To this solution, 2 ml of 5 stock collagenase (Worthington CLS-II 1,000 units/ml in HL-1) and 1 ml of hyaluronidase (Sigma Type III, 5 mg/ml in HL-1) was added for overnight digestion at 37°C with mechanical agitation. The following morning cartilage 10 remnants were diluted with 10 ml of fresh media and gently vortexed (3 x 1 minutes) to release chondrocytes from the remaining extracellular matrix.

Chondrocytes were then separated from tissue debris by gravity filtration through a sterile Falcon cell strainer unit (70 μ m) and sedimented at 600 x g for 10 minutes in 15 a clinical centrifuge. Cell viability was greater than 95%. Next, chondrocytes were diluted in DMEM + 10% FBS for plating in either 12 or 24 well plastic culture dishes at a density of 1-2 x 10⁵ cells/cm² in 1 ml of growth media and grown at 37°C in a 95% air, 5% CO₂ atmosphere.

20 Chondrocytes were initially seeded in FBS to promote adherence and to stimulate cell division. Ascorbate (50 μ g/ml, Sigma Chemical, St. Louis, MO) was added fresh at plating and at each feeding, generally every 72-96 hours.

On day 7, neocartilage cultures were weaned of serum 25 (5%) and remained 100% serum-free (i.e., in HL-1) from day 10 onward. HL-1 is a chemically defined serum-free media containing insulin-transferrin-selenium-complex as its only source of protein. However, other serum-free media high in arginine and supplemented with insulin-transferrin-selenium 30 may be substituted for HL-1. Where indicated, conditioned media from fetal culture was added to 20% at all media changes to enhance neocartilage formation from infant chondrocytes.

Under the described serum-free conditions, immature 35 chondrocytes displayed tremendous proliferative capacity, as well as the ability to synthesize and deposit an

insoluble hyaline cartilage matrix. A gross representation of day 90 neocartilage tissue is shown in FIG. 1. The neocartilage is rigid, yet malleable and was easily removed from culture vessels after day 20 using forceps. This 5 material was strong enough to hold suture material after day 30 of culture and was amenable to surgical implantation at day 40.

Neocartilage cultures were maintained under said conditions and harvested for biochemical and histological analyses between day 1-60 and again at days 90 and 120. 10 Parallel cultures were maintained in DMEM + 10% fetal bovine serum for comparison.

EXAMPLE 2

Biochemical Assessment of Neocartilage Formation -

15 Neocartilage formation was assessed by colorimetric analyses of sulfated glycosaminoglycan (S-GAG) and hydroxyproline (OH-proline), general measures of proteoglycan and collagen synthesis, respectively. Neocartilage disks were lyophilized and digested 18 hrs at 20 56°C in 500 μ l of 0.1 M sodium acetate buffer (pH 5.6), containing 5mM Na₄EDTA, 5mM L-cysteine, and 125 μ g/ml papain. The digests were cooled to room temperature for determination of S-GAG, OH-proline, and DNA content.

25 Sulfated-GAG and the OH-proline content of papain digested material were determined at the indicated times via microplate colorimetric procedures adapted from Farndale et al., *Biochim Biophys Acta* 883: 173-177 (1986), and Stegemann and Stalder, *Clin Chim Acta* 18: 267-273 30 (1967), respectively. Chondroitin-6-sulfate (Calbiochem) and cis-4-hydroxy-L-proline (Sigma) were used as standard.

DNA content was estimated by fluorometric analysis using a CytoFluor microplate reader. Bisbenzamide (Hoechst 33258, Sigma Chemical Co., St. Louis, MO) was dissolved at 1 mg/ml in water and a working stock diluted further to 0.1

μ g/ml in 10 mM tris-HCl, pH 7.4, containing 0.1 M NaCl and 10 mM EDTA.

Ten, 20- and 50-fold dilutions of each sample were prepared and 10 μ l aliquots assayed by mixing with 100 μ l of dye solution. Fluorescence was read (excitation wavelength = 355 nm; emission wavelength = 460 nm) and DNA content determined from a standard curve that was constructed using herring sperm DNA (Gibco BRL).

Fetal chondrocytes displayed a rapid proliferative phase of cell growth (FIG. 2) and matrix deposition when grown under serum-free conditions, generating tissue that was 1.5-2.0 mm thick and weighing 300-400 mg (3.8 cm² dishes) at day 120. In contrast, supplementation with 10% serum reduced total S-GAG and hydroxyproline content by 80-90% at day 30 (FIG. 3). Furthermore, the structural integrity of these samples (+ 10% serum) was very poor. These samples could not be taken past day 30 of culture without shrinking and balling up. Day 28 neocartilage with 10% serum for an additional 28-day period causes >90% loss in matrix aggrecan (FIG. 4). This effect was titratable, thereby suggesting that either specific components of serum degrade cartilage matrix directly or, alternatively, that serum induces synthesis and/or activation of chondrocyte-derived matrix metalloproteinases.

The potential for neocartilage formation from pre-adolescent and adult articular chondrocytes is depicted in Table I and appears to correlate with skeletal development. Neocartilage formation was not recapitulated in these experiments using articular cartilage obtained from post-adolescent subjects.

TABLE I. Effect of Donor Age on Neocartilage Potential

Donor Age	Time in Culture (days)	S-GAG (μg)
Fetal #1	30	3,583 ± 106
Fetal #2	60	9,126 ± 30
Fetal #3	120	7,750 ± 125
Infant (1d)	25	6,853 ± 79
Infant (8 mo)	300	9,664 ± 313
12 y	30	1,102 ± 117
20 y	30	107 ± 15
27 y	30	46 ± 8
36 y	30	53 ± 13
43 y	30	31 ± 2

High density cultures were established in 12 well clusters as described, and neocartilage formation was allowed to proceed until time of harvest. Triplicate samples were assayed for total S-GAG using dimethyl methylene blue.

Characterization of the morphological appearance and biochemical composition of the tissue revealed an ultrastructural organization that was hyaline in nature and nearly indistinguishable from native articular cartilage. 5 Chondrocytes were constrained to individual lacunae and were encased in an extensive extracellular matrix which stained metachromatically for aggregating proteoglycan (safranin-O) and collagen (pentachrome) (FIG. 5). Moreover, the pentachrome technique failed to identify 10 elastic fibers previously shown to be present in cultures of bovine articular chondrocytes maintained in the presence of serum [Lee et al., *Dev. Biol.* 163: 241-252 (1994)].

Fibrocartilage contamination, a problem typically encountered when articular chondrocytes are cultivated using traditional cell culture methods (i.e., media containing 10% serum), could not be identified in 5 pepsinized extracts of neocartilage material by Western analysis (chemiluminescence detection) or by transmission electron microscopy (TEM) following tissue fixation. The dominant collagen identified by TEM consisted of 20 nm fibrils, while beaded filaments, indicative of type VI 10 collagen, were localized to the lacunae (FIG. 6). Type I collagen fibers typically display a fibril diameter of 100 nm. Western analysis confirmed the presence of type II collagen as the dominant (90%) isotype, and further 15 identified minor cartilage-specific collagens such as collagen types IX and XI (FIG. 7).

Cross reactivity with antibodies to collagen types III and X were also negative in neocartilage, but were reactive in collagen preparations obtained from adult articular cartilage. Thus, the composition of the collagen contained 20 within the neocartilage tissue produced by the method of the invention is indistinguishable in appearance from the starting material from which the cells originated; however, it differs significantly from that of adult and 25 osteoarthritic articular cartilage in that collagen types I, III and X were not detected.

Collagens of the neocartilage matrix can be isolated via pepsinization and neutral salt precipitation (Miller, EJ and Rhodes RK; 1982, *Methods of Enzymology* 82:33-64) for 30 use in the production of cartilage biomatrices. The culture conditions described herein are ideal for producing the normal complement and ratio of cartilage collagens, which include but are not limited to types II, VI, IX, and XI.

EXAMPLE 3

Model systems for studying articular cartilage disease and articular cartilage response to natural and synthetic compounds. Neocartilage cultures were established in 24 or 5 48 well plastic dishes (Corning) as described above (Example 1) and grown to day 30. The hyaline cartilage matrix was then stimulated to undergo autolytic degradation following 30 day activation with increasing concentrations of a variety of cytokine and/or inflammatory agents, 10 including IL-1, IL-6, IL-17, TNF- α , LPS, and phorbol ester. Culture media were collected every 48 hours and subsequently changed by the addition of fresh media \pm inflammatory stimuli.

15 Cultures were terminated and the biochemical composition of the neocartilage matrix that remained was analyzed as described previously. Parallel samples were processed for light and transmission electron microscopy for histological evaluation of extracellular matrix components.

20 Conditioned media were thawed and identification of chondrocyte-derived metalloproteinases assessed by zymogen substrate gel electrophoresis, as well as Western analysis following SDS-PAGE. Further studies examined the effect of activating agents on synthesis of S-GAG and collagen via 25 radiolabeled incorporation.

Resorption of neocartilage material was readily apparent by gross examination between day 20-25 of 30 stimulation (FIG. 8). Resorption was characterized by a reduction in the diameter of the neocartilage material and its retraction upon removal from the culture vessel, indicating that the structural integrity of the tissue was significantly compromised.

Histological evaluation (i.e., safranin-O and 35 pentachrome staining) of treated and control material revealed a marked reduction in the S-GAG and collagen content of treated samples (FIG. 9). TEM studies also

demonstrated a significant alteration in the morphological appearance of the chondrocytes to more of a fibroblast/macrophage lineage (i.e., numerous microvillus projections were identified on the surface of flattened, spindle shaped 5 cells), whereas chondrocytes in untreated controls maintained their rounded phenotype (not shown).

The OH-proline and S-GAG content of treated neocartilage disks were reduced by 20-85% depending on the dose and identity of the activating agent (Table II). Both 10 zymogram and Western analysis identified collagenolytic and casienase activities that were upregulated in the presence of activating agent alone (FIG. 10).

TABLE II. Hydroxyproline content of tissue matrix following chronic cytokine treatment

Condition	OH-proline content of tissue (pmoles)*	
Control	1710±251	
+ 50 mU plasminogen†	1648± 72	
IL-1 β	0.1 (ng/ml)	572±105
	1.0	541± 16
	5.0	501± 48
+ 50 mU plasminogen		460± 16
TNF- α	1.0	403
	5.0	355

*Samples were lyophilized and digested with papain prior to hydrolysis for determination of OH-proline content via HPLC analysis. †Human plasminogen was added to enhance the activation of latent MMPs via the plasminogen activator/plasmin cascade.

Phorbol ester specifically induced synthesis of gelatinase B, whereas the cytokine treatments resulted in the production of numerous bands (9-11) on substrate gels, three of which were identified as collagenase 1, 2 and 3 by 5 Western immunoblotting (FIG. 11). Each of these enzymes are implicated in arthritic disease.

This system is unique in that the anabolic and catabolic properties of *normal human chondrocyte* metabolism can be examined, under defined serum-free conditions. It 10 is clear that the described model of neocartilage formation will facilitate the development and evaluation of pharmacological agents to protect the cartilage matrix from arthritic destruction.

EXAMPLE 4

15 Surgical Repair of Rabbit Articular Cartilage via Transplantation of Rabbit Neocartilage Allografts.

Neocartilage allografts were produced from 10-day neonates as described in Example 1. Extreme care was taken to eliminate the use of vascularized epiphyseal cartilage 20 during tissue preparation.

Neocartilage implants were grown to day 30, fixed and stained for histological evaluation, and further extracted for analysis of cartilage specific macromolecules. This procedure yielded hyaline tissue that was enriched in both 25 cartilage specific collagens and glycosaminoglycans (Table III.)

TABLE III. Composition of Rabbit Neocartilage

Component	Relative Abundance
<i>Collagen</i>	
type I	-
type II	+++
type IX	+
type XI	+
Aggrecan	14,365 ± 410 µg

High density cultures were established in 12 well clusters as described, and neocartilage formation was allowed to proceed until harvest on day 40. Triplicate samples were assayed for total S-GAG using dimethyl methylene blue. Isotyping of collagen was performed via electrophoresis on 6.5% SDS-polyacrylamide gels under reduced conditions.

Eighteen (18) skeletally mature (30 wk) male New Zealand White rabbits were divided into three groups to assess the healing potential of transplanted neocartilage at 1, 3, 6 and 12 weeks post-operatively. Rectangular defects of approximately 3 mm in width, spanning the girth of the medial femoral condyle (5mm), were created surgically in both knees (FIG. 12). Violation of subchondral bone was avoided during this procedure.

Sterile neocartilage implants (day 35-45 *in vitro*) were subsequently cut to size and sutured into the experimental defect (right side) using 7-0 vicryl suture, anchoring neocartilage to the medial and lateral

perichondria, following addition of tissue transglutaminase as described in Jurgensen et al., *J. Bone Joint Surg.* 79-A, 185-193 (1997). Unfilled defects (left side) were allowed to heal intrinsically and served as the contralateral sham 5 control. Arthrotomies were repaired using 4-0 vicryl suture and animals were permitted free cage activity. Oral analgesic was provided for 24 hours post-operatively as needed for pain.

The animals showed excellent tolerance of the surgical 10 procedures, displaying normal ambulation and increased appetite within 24 hours post-operatively. Gross examination of the experimental defects harvested at six weeks revealed good adherence of grafts to surrounding tissue, whereas unfilled defects remained unfilled 15 (FIG.13).

EXAMPLE 5

Immunological Assessment of Allograft Rejection - A one-way mixed leukocyte reaction (MLR) was set up in which chondrocytes, acting as the stimulator population, were 20 first gamma-irradiated in order to block their proliferative potential. Allogeneic leukocytes, obtained from either peripheral blood or buffy coats (American Red Cross) were then passed over a Ficoll gradient. This population of mononuclear leukocytes was counted and 25 subsequently co-cultured with chondrocytes, having first been isolated from day 30-45 neocartilage allografts. Adult cells were also isolated from day 30 cultures which were grown under conditions identical to the neocartilage.

Proliferation of non-irradiated leukocytes was 30 determined on day 7, following a 24 hr pulse with tritiated thymidine (Amersham, 1 μ Ci/ml) (Abbas, AK, et al. 1991 *In Cellular and Molecular Immunology*, pp. 320-322). Culture plates were frozen, the cells lysed in water, and the nuclear DNA aspirated and bound to glass filtermats using 35 an automated cell harvester. Filtermats were then dried

and counted in a Wallac MicroBeta scintillation counter. Chondrocytes isolated from day 30-45 neocartilage failed to generate an MLR response that would indicate a cross match (FIG. 14B), while the positive controls showed a 19-fold 5 increase in proliferation.

These data support the concept that chondrocytes are immunologically privileged. Although chondrocytes are reported to present MHC class II antigens on their cell surface [Elves, *J. Bone Joint Surg.*, 56B:178-185 (1974); 10 Jahn et al., *Arth Rheum* 30:64-74 (1987); and Jobanputra et al., *Clin. Exp. Immunol.* 90:336-344 (1992)], proliferation of the responder leukocyte population was not detected in three separate assays involving at least twelve (12) different neocartilage samples. From an immunological 15 perspective, these experiments indicate that the present approach to cartilage repair (e.g., allograft transplantation) is feasible.

Additional studies examining the co-stimulatory function of chondrocytes in a T-cell based assay (Abbas, 20 AK, et al. 1991, *In Cellular and Molecular Immunology*, pp. 320-322) were also negative, indicating that co-stimulatory molecules, probably B7.1 (CD80) and B7.2 (CD86) are not normally expressed by chondrocytes (FIG. 15). Thus, applicant has discovered appropriate culture conditions 25 which permit transplantation of neocartilage into allogeneic recipients.

EXAMPLE 6

Overlaying of chondrocytes to increase the thickness and structural integrity of neocartilage - Rabbit and human 30 chondrocytes were isolated, seeded into 12-well dishes and grown to day 10 as described above. During the initial plating of these cultures, 1.4×10^7 cells were reserved for plating in 100 mm dishes. Cells were subsequently released from the culture surface on day 10 using the 35 collagenase/hyaluronidase procedure described in Example 1.

Chondrocytes were filtered, counted and resuspended in a 1:1 mixture of DMEM + 10% FBS/HL-1, containing ascorbate, at a density of 0.5×10^6 /ml. Day 10 cultures (12-well plates) were overlayed with 1 ml of the cell suspension to 5 increase the thickness and structural integrity of the neocartilage grafts. The cultures were maintained in the 1:1 mix of DMEM/HL-1 from day 13-17, after which they were 10 grown in HL-1 media until harvest at day 40. Total S-GAG in the neocartilage matrix were quantified as described above. FIG. 16 shows that the overlaying procedure increased total S-GAG content by approximately 50%, and as a result increased the rigidity of the neocartilage matrix.

EXAMPLE 7

Isolation and Characterization of Neocartilage Proteoglycan - Neocartilage cultures were established and grown to day 35 as described in Example 1. Newly synthesized proteoglycans were metabolically labeled for 72 hrs using carrier-free [35 S]-sodium sulfate (55 μ Ci/ml, Amersham, supra). Following three washes with PBS to 20 remove unincorporated label, the proteoglycans of the neocartilage matrix were extracted in 4M guanidine and precipitated in ethanol. Unlabeled native proteoglycans were also extracted from the articular cartilage of a 12-yr female and 43-yr male for comparison. Twenty (20) μ g of S-GAG were loaded and separated on 1.2% agarose gels 25 according to the method of Bjornsson, *Anal. Biochem.*, 210: 292-298 (1993), (FIG. 17).

Greater than 95% of the labeled material was identified as aggrecan, as judged by molecular weight. 30 However, it was noted that this material was of higher molecular weight than the aggrecan found in pre-teen and adult tissue, indicating that the aggrecan monomers were more highly glycosylated. A minor band with 35 electrophoretic mobility identical to that of native decorin was also observed in the neocartilage matrix.

Biglycan, present as a minor component of native articular cartilage, was not identified via radiolabel incorporation in 6 replicates of neocartilage. Only 12-15% of the total radiolabeled S-GAG could be recovered in culture supernatant, generating the same profile as that shown here.

Thus, the composition of neocartilage proteoglycan differs from that of mature articular cartilage in two distinct ways. First, biglycan was not identified as a component of the neocartilage matrix; and second, the innate composition of neocartilage proteoglycan appears to be more highly glycosylated, resulting in a high molecular weight aggrecan. It is believed that this aggrecan may play a role in tissue growth and repair by binding specific growth factors with greater avidity than adult aggrecan.

Purification of this material for testing as a wound healing agent is relatively easy and inexpensive. High molecular weight aggrecan bands identified on 1.2% agarose gels were removed and eluted to purity using a BioRad electroelution device. Preliminary studies demonstrate that a 200 mg neocartilage disk yielded 3-4 mg of high molecular weight aggrecan.

EXAMPLE 8

Role of heparin binding proteins in neocartilage formation: Identification of two new members of the TGF- β Superfamily - Fetal chondrocytes were grown as described above and subdivided into three groups on day 10 to investigate the effect of heparin on neocartilage formation. In low doses, heparin is known to increase the activity of certain growth factors, for example the fibroblast growth factor (FGF) family of related proteins, by acting as a co-factor, whereas greater amounts of heparin will strip away certain growth factors from the extracellular matrix and thereby impede tissue repair.

Sterile heparin was added to the media at a final concentration of 0.2, 2.0, and 20 μ g for the duration of the culture period (i.e. from day 10-28). Media were exchanged every 3-4 days and recovered for electrophoretic analysis of secreted proteins. Cell layers were removed and the S-GAG (FIG. 18A), hydroxy proline (FIG. 18B), and DNA content quantitated as before (FIG. 18). The highest concentration of heparin caused a severe defect (60% inhibition in S-GAG and 33% in OH-proline) in matrix deposition. This effect was also evident in the 2 μ g/ml treatment group, but was much less severe.

When these heparin binding proteins are then extracted from the neocartilage matrix using procedures adapted from Chang et al., approximately 10 proteins showing a molecular mass of less than 60 kDa are visible on a 4-20% gradient Tris/Tricine polyacrylamide gel (FIG. 19). Western blotting using antibodies from the NIH have shown that cartilage derived morphogenetic protein-1 and -2 (CDMP-1 and -2) are present, as was connective tissue derived growth Factor (CTGF) (not shown).

EXAMPLE 9

Serum-free culture depletes neocartilage of precursor fatty acids for eicosanoid synthesis - Adkisson et al.,

FASEB J 5: 344-353 (1991), discovered high concentrations of 20:3 n-9 eicosatrienoic acid and low concentrations of n-6 polyunsaturated fatty acids (PUFA) in normal, rapidly growing cartilages of several vertebrates, a biochemical hallmark of essential fatty acid deficiency. Because the n-6 fatty acids, in particular arachidonic acid (20:4 n-6), are key mediators of inflammation and transplant rejection (Schreiner et al., *Science* 240: 1032-1033 (1988), the fatty acid composition of neocartilage grafts were characterized 10 during a 28-day time course *in vitro*.

Total cellular lipids and the phospholipid fraction were isolated as described in Adkisson et al., supra. Pentafluorobenzyl ester derivatives of the free fatty acids obtained from the phospholipid fraction were prepared for 15 microanalysis by capillary gas chromatography using a SP-2380 fused silica column (Supelco Inc., Bellefonte, PA). The gas chromatograph (HP model 5890) was held at 160°C for 2 min., temperature programmed at 10°C/min to 200°C, and maintained at this temperature for an additional 10 min. 20 Both the injector and the electrochemical detector temperatures were set at 225°C. Derivatized fatty acids were identified by co-migration with authentic standards, while unusual fatty acids were characterized by their fragmentation pattern using mass spectrometry analysis of 25 their picolinyl ester derivative as described previously (Adkisson et al., 1991). Percent composition of individual fatty acids was determined by integration using Hewlett-Packard model 3393A integrator.

FIG. 20 illustrates that essential fatty acids, a component of the culture media (i.e., 5-10% FBS from day 1-10), are rapidly incorporated into the phospholipid stores of isolated chondrocytes. Moreover, it is clear that once the cultures are switched to and maintained in serum-free HL-1 media (closed circles), the native complement of fatty acids is restored, such that low levels of the n-6 PUFAs are detected. The n-6 fatty acids, shown in the upper

three panels, continue to accumulate in chondrocyte phospholipids when the neocartilage cultures are maintained in serum-containing media (open circles).

FIG. 21 is a mass chromatogram of the dominant polyunsaturated fatty acid identified in neocartilage phospholipids (i.e. 20:3 n-9 eicosatrienoic acid) at day 28 of culture. The fragmentation pattern matches that of authentic 20:3 n-9 eicosatrienoic or Mead Acid.

It is unclear whether enrichment in n-9 fatty acids reduces antigen expression of MHC class II molecules or B7 co-stimulatory molecules which are required to establish immunogeneity in allograft rejection. The literature does support the fact that a dearth of n-6 PUFA modulates the infiltration of inflammatory cells by inhibiting leukotriene formation (Cleland et al., 1984, *Lipids* 29:151-155, and Schreiner et al., 1988, *supra*). This in turn protects organs from possible transplant rejection.

In summary, the novel serum-free culture system used to produce neocartilage tissue may facilitate allogeneic transplantation of the neocartilage by regulating chondrocyte immunogenicity, as well as the elaboration of inflammatory eicosanoids/cytokines.

EXAMPLE 10

Preparation of neocartilage/demineralized bone composites-

Day 60 neocartilage cultures were enzymatically dispersed as described in Example 1 one million chondrocytes were then seeded onto samples of demineralized allograft bone (Lambone™, 100-300 μm thick) which were first trimmed to accomodate in vitro culture in 12 well clusters. Lambone™, obtained from Pacific Coast Tissue Bank, Los Angeles, CA, was washed extensively in culture media to remove residual ethylene oxide gas used during tissue processing.

Neocartilage formation on demineralized allograft bone was allowed to proceed to day 28 as described herein. Neocartilage/Lambone composites were then rinsed and fixed overnight in 10% neutral buffered formalin for 5 morphological examination via pentachrome staining.

FIG. 22A and B illustrate the morphologic appearance of neocartilage/Lambone™ composites following pentachrome staining. Magnification: 22A, 100x; 22B 200x.

In view of the above, it will be seen that the several 10 objects of the invention are achieved.

As various changes could be made in the above compositions and methods by the person skilled in the art after reading the present disclosure without departing from the spirit and scope of the invention, it is intended that 15 all matter contained in the above description shall be interpreted as illustrative of the claimed invention and not in a limiting sense.

With reference to the use of the word(s) "comprise" or "comprises" or "comprising" in the foregoing description and/or in the following claims, unless the context requires 20 otherwise, those words are used on the basis and clear understanding that they are to be interpreted inclusively, rather than exclusively, and that each of those words is to be so interpreted in construing the foregoing description and/or the following claims.



The claims defining the invention are as follows:

1. A biological material comprising cartilage containing membrane phospholipids enriched in Mead acid.
2. A biological material as set forth in claim 1 wherein the Mead acid content of said membrane phospholipids comprises at least about 2% of the total fatty acid content of said membrane phospholipids.
3. A biological material as set forth in claim 1 wherein the Mead acid content of said membrane phospholipids comprises between about 2.5% and 10% of the total fatty acid content of said membrane phospholipids.
4. A biological material comprising cartilage containing membrane phospholipids depleted in linoleic acid.
5. A biological material as set forth in claim 4 wherein the linoleic acid content of said membrane phospholipids comprises less than about 0.5% of the total fatty acid content of said membrane phospholipids.
6. A biological material as set forth in claim 4 wherein the linoleic acid content of said membrane phospholipids comprises less than about 0.2% of the total fatty acid content of said membrane phospholipids.
7. A biological material comprising cartilage containing membrane phospholipids depleted in arachidonic acid.
8. A biological material as set forth in claim 7 wherein the linoleic acid content of said membrane



phospholipids comprises less than about 0.5% of the total fatty acid content of said membrane phospholipids.

9. A biological material as set forth in claim 7 wherein the arachidonic acid content of said membrane phospholipids comprises less than about 0.2% of the total fatty acid content of said membrane phospholipids.

10. A biological material as set forth in any one of claims 1 to 9 wherein said cartilage is substantially free of endothelial, bone and synovial cells.

11. A biological material as set forth in any one of claims 1 to 10 wherein said cartilage has a S-GAG content of at least about 400 mg/mg of OH-proline.

12. A biological material as set forth in any one of claims 1 to 10 wherein said cartilage has a S-GAG content of from about 600mg to about 2500 mg/mg of OH-proline.

13. A biological material as set forth in any one of claims 1 to 12 wherein said cartilage is substantially free of type I, III and X collagen.

14. A biological material comprising cartilage containing a matrix substantially free of biglycan.

15. A biological material comprising cartilage enriched in high molecular weight aggrecan.

16. A biological material as set forth in claim 15 wherein the high molecular weight aggrecan comprises at least about 80% of the total proteoglycan content of said cartilage.



17. A biological material as set forth in claim 15 wherein the high molecular weight aggrecan comprises about 90% of the total proteoglycan content of said cartilage.

18. A biological material comprising cartilage characterized as follows:

- (a) containing membrane phospholipids enriched in Mead acid and depleted in linoleic and arachadonic acid;
- 5 (b) being enriched in high molecular weight aggrecan;
- (c) being substantially free of endothelial, bone and synovial cells;
- (d) being substantially free of biglycan; and
- 10 (e) being enriched in high molecular weight aggrecan.

19. A biological material as set forth in claim 18 wherein the cartilage is further characterized by having multiple layers of cells, said cells surrounded by a substantially continuous insoluble glycosaminoglycan and collagen-enriched hyaline extracellular matrix.

20. A composition comprising neocartilage and being essentially free of non-cartilage materials characterized by having multiple layers of cells, said cells surrounded by a substantially continuous insoluble glycosaminoglycan and collagen-enriched hyaline extracellular matrix.

5 21. The composition of claim 20, wherein said neocartilage is mammalian or avian neocartilage.

22. The composition of claim 21, wherein said neocartilage is human neocartilage.



23. The composition of claim 21, wherein said neocartilage is derived from a transgenic animal genetically engineered for resistance to immune-mediated xenograft rejection.

24. The composition of claim 21, wherein said transgenic animal is porcine.

25. The composition of claim 20, wherein said neocartilage is articular neocartilage.

26. The composition of claim 20, wherein said neocartilage is hyaline neocartilage.

27. The composition of claim 20, wherein said neocartilage is produced using immature chondrocytes.

28. A biological material comprising essentially purified cartilage-specific macromolecules.

29. A biological material as set forth in claim 28 wherein the material is substantially free of types I, III and X collagen.

30. A biological material as set forth in claim 29 wherein the macromolecules are selected from one or more of the group consisting of types II, VI, IX, and XI collagen and aggrecan.

31. A biological material as set forth in claim 28 wherein the macromolecules consist essentially of high molecular weight aggrecan.

32. A biological material as set forth in claim 28 wherein the macromolecules consist essentially of type II collagen.

33. A biological material as set forth in claim 28 wherein the macromolecules consist essentially of type VI collagen.

34. A biological material as set forth in claim 28 wherein the macromolecules consist essentially of type IX collagen.

35. A biological material as set forth in claim 28 wherein the macromolecules consist essentially of type XI collagen.

36. A conditioned growth medium adapted for use in growing cartilage cell cultures comprising heparin-binding growth factors, at least one of which is a cartilage-derived morphogenetic protein.

37. A method for growing neocartilage comprising: isolating chondrocytes; adhering said chondrocytes to a surface using means effective to produce a cell culture; and growing said cell culture in a substantially serum-free growth media to produce neocartilage.

38. A method for growing neocartilage as set forth in claim 37 wherein said adhering means comprise growing said chondrocytes in a growth media containing an amount of serum effective to allow adherence of said chondrocytes.

39. The method of claim 38, wherein the method further comprises adding to said substantially serum-free cell culture an amount of conditioned growth media effective to enhance neocartilage formation.

40. The method of claim 38, wherein the method further comprises adding ascorbate to said cell culture.

41. The method of any one of claims 37 to 40, wherein said chondrocytes are immature chondrocytes.

42. The method of any one of claims 37 to 41, wherein said chondrocytes are human chondrocytes.

43. The method of any one of claims 39 to 42, wherein said conditioned growth media is between approximately 5 percent and 30 percent of said substantially serum-free growth media.

44. The method of any one of claims 39 to 42, wherein said conditioned growth media is approximately 20 percent of said substantially serum-free growth media.

45. The method of claim 37, wherein said substantially serum-free growth media comprises growth factors for the proliferation of said chondrocytes.

46. The method of claim 39, wherein said conditioned growth media comprises growth factors for the proliferation of said chondrocytes.

47. The method of claim 46, wherein said growth factors are autocrine factors.

48. The method of claim 39, wherein said conditioned growth media contains factors for the differentiation of said chondrocytes.

49. The method of claim 39, wherein said conditioned growth media contains factors for the anti-invasion of non-chondrocytic cells.

50. A composition comprising the neocartilage produced by the method of any one of claims 37 to 49.



51. A set of implant materials comprising an implant containing a reparative amount of the 5 neocartilage produced by the method of any one of claims 37 to 49 and means for implanting and adhering the neocartilage in a target tissue locus.

52. A set of implant materials comprising an implant containing a reparative amount of a biological material comprising cartilage containing membrane phospholipids enriched in Mead acid and means for 5 implanting and adhering the neocartilage in a target tissue locus.

53. A method of repairing defective cartilage in vivo comprising surgically implanting and adhering the implant of claim 52.

54. The method of claim 53, wherein said adhering means comprise sutures.

55. The method of claim 54, wherein said adhering means further comprises enzymatic cross-linking or chemical tissue welding use in combination with sutures.

56. The method of claim 53, wherein said implant is adhered to adjoining natural cartilage by means of a sutureless attachment.

57. The method of claim 56, wherein said means of sutureless attachment comprise means selected from the group consisting of chemical tissue welding or enzymatic cross-linking.



58. A method for producing a conditioned growth media comprising: isolating chondrocytes; producing a cell culture by growing said chondrocytes in a growth media containing an amount of serum effective to allow adherence of said chondrocytes; replacing said growth media containing an amount of serum with a substantially serum-free growth media after the beginning time interval to produce a substantially serum-free cell culture; growing said substantially serum-free cell culture to produce conditioned growth media; and extracting or concentrating said conditioned growth media from said substantially serum-free cell culture.

59. The conditioned growth media produced by the method of claim 58.

60. The conditioned growth media of claim 59, wherein said conditioned growth media is produced using immature chondrocytes and which comprises growth factors which stimulate the proliferation and differentiation of chondrocytes in a cell culture.

61. The conditioned growth media of claim 60, wherein said growth factors are autocrine factors.

62. A method for producing cartilage derived compounds comprising: isolating chondrocytes; producing a cell culture by growing said chondrocytes in a growth media containing an amount of serum effective to allow adherence of said chondrocytes; replacing said growth media containing an amount of serum with a substantially serum-free growth media after the beginning time interval to produce a substantially serum free cell culture; growing said substantially serum-free cell culture to produce isolated neocartilage; and extracting cartilage derived compounds from said neocartilage.

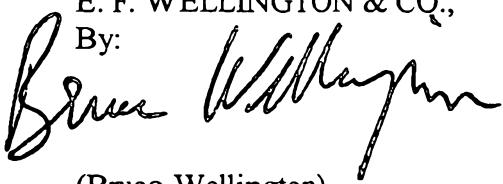


63. A method for screening a pharmaceutical for its capacity to modulate arthritic disease comprising co-culturing the composition of any one of claims 20 to 27, or 50 with said pharmaceutical in an amount and under conditions effective for determining whether characteristic indications of arthritic modulation are observed in said composition.

DATED this 7 day of November 2001

BARNES JEWISH HOSPITAL,
By its Patent Attorneys,
E. F. WELLINGTON & CO.,

By:



(Bruce Wellington)



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FIG. 1A

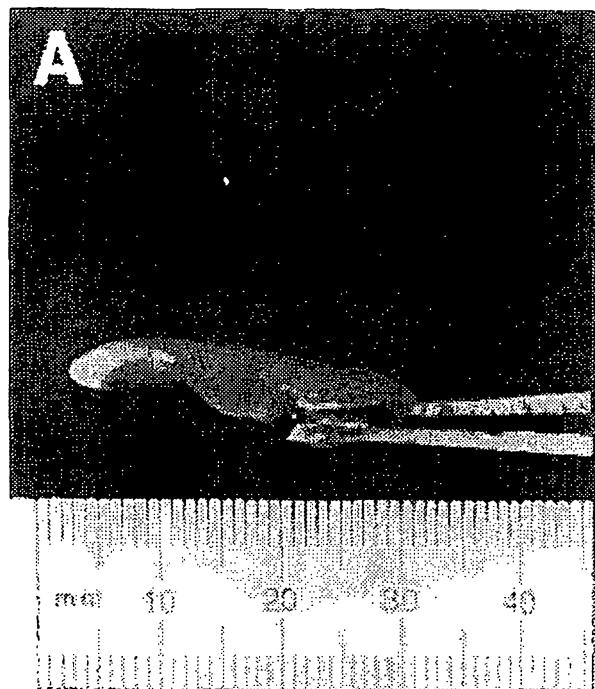
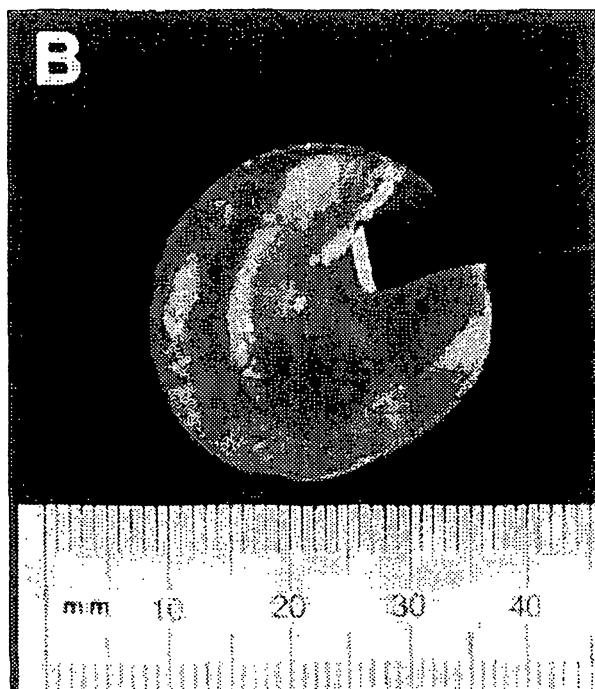


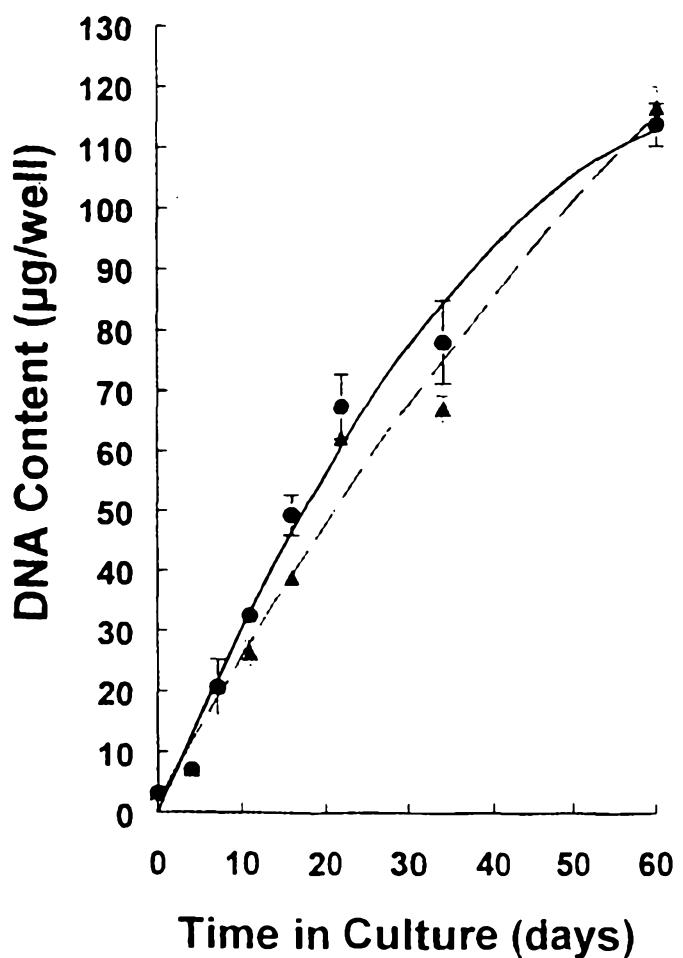
FIG. 1B



SUBSTITUTE SHEET (RULE 26)

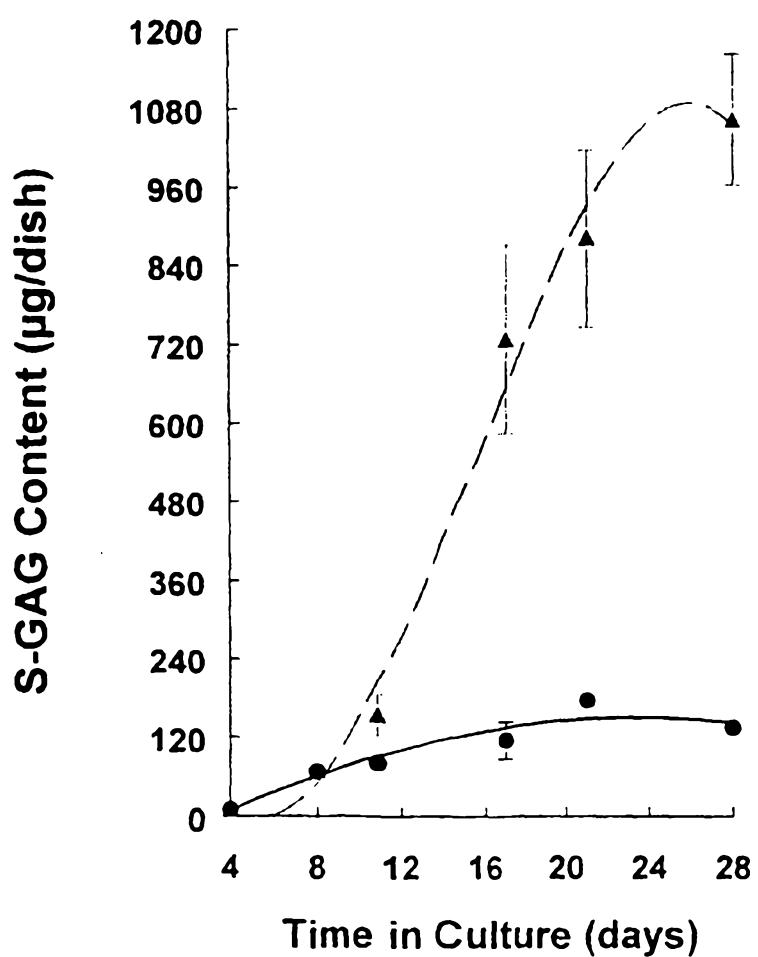
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FIG. 2



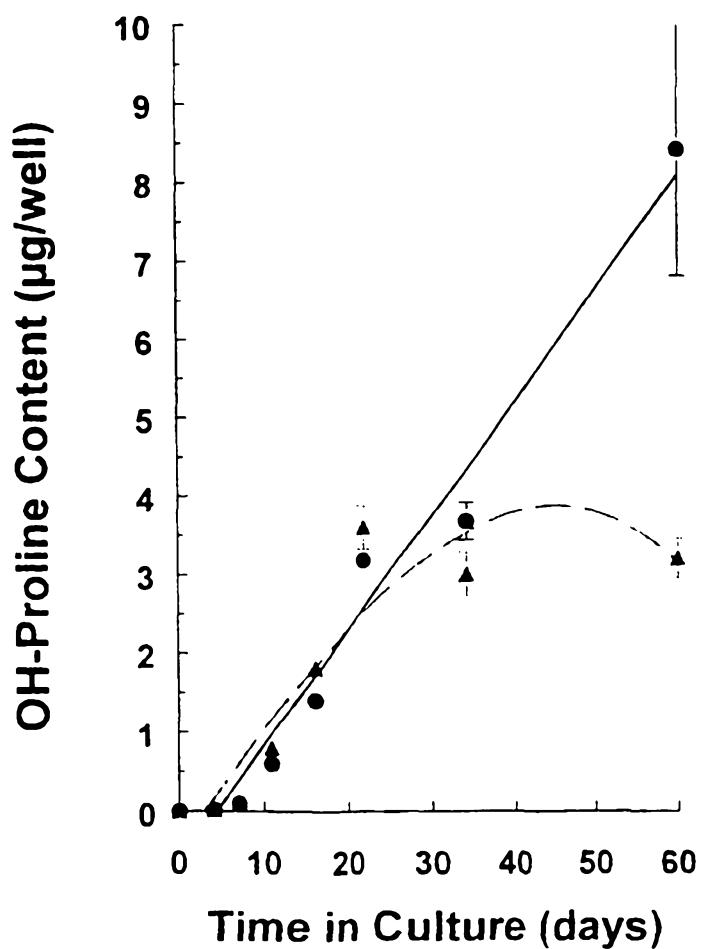
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FIG. 3A



4 / 25

FIG. 3B



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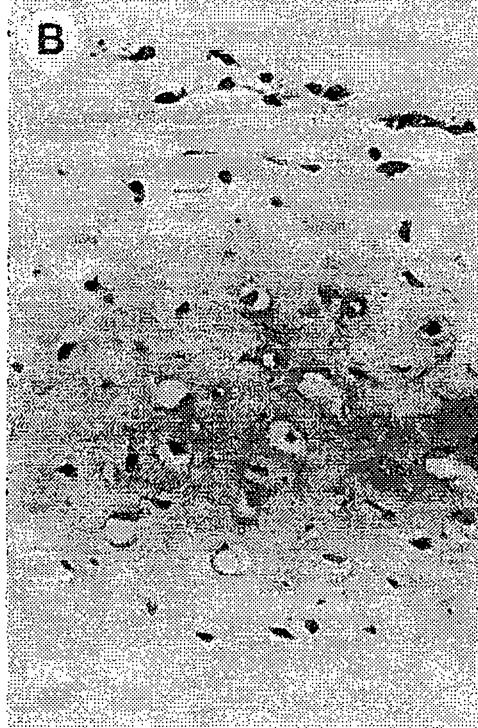


FIG. 5A

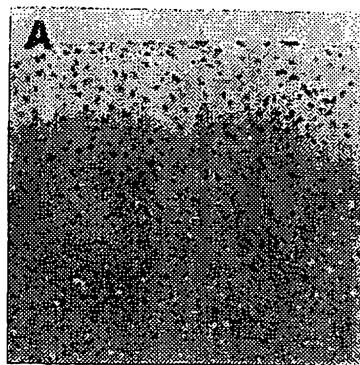


FIG. 5B

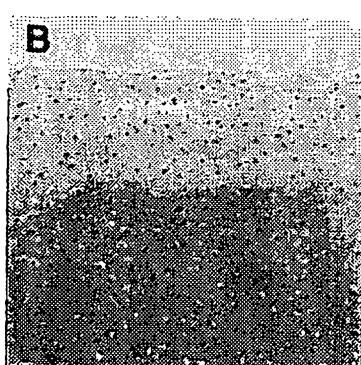


FIG. 5C

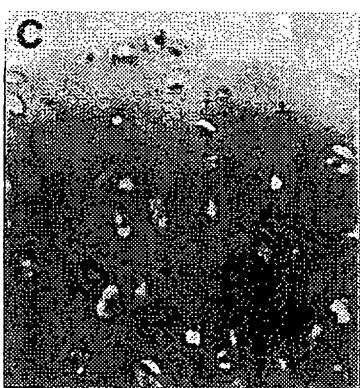


FIG. 5D



FIG. 5E



FIG. 5F

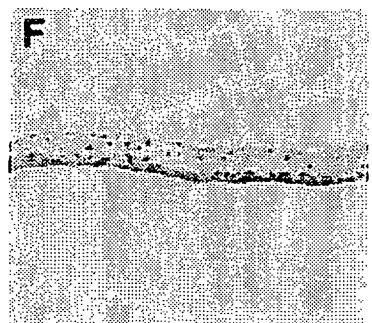


FIG. 6A



FIG. 6B

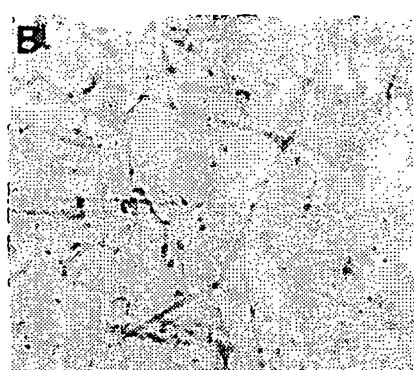


FIG. 6C

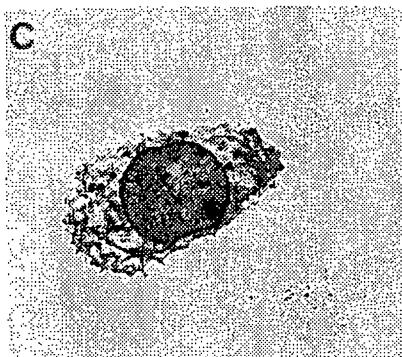


FIG. 6D

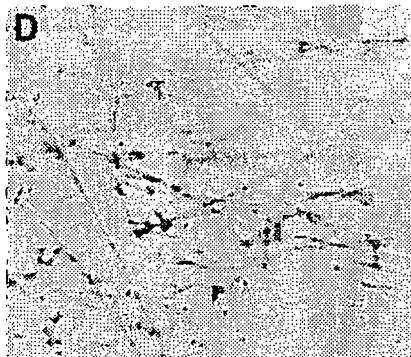


FIG. 6E



FIG. 6F

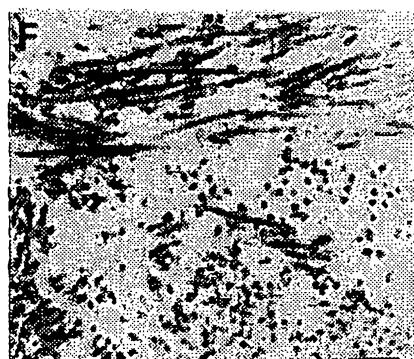


FIG. 7

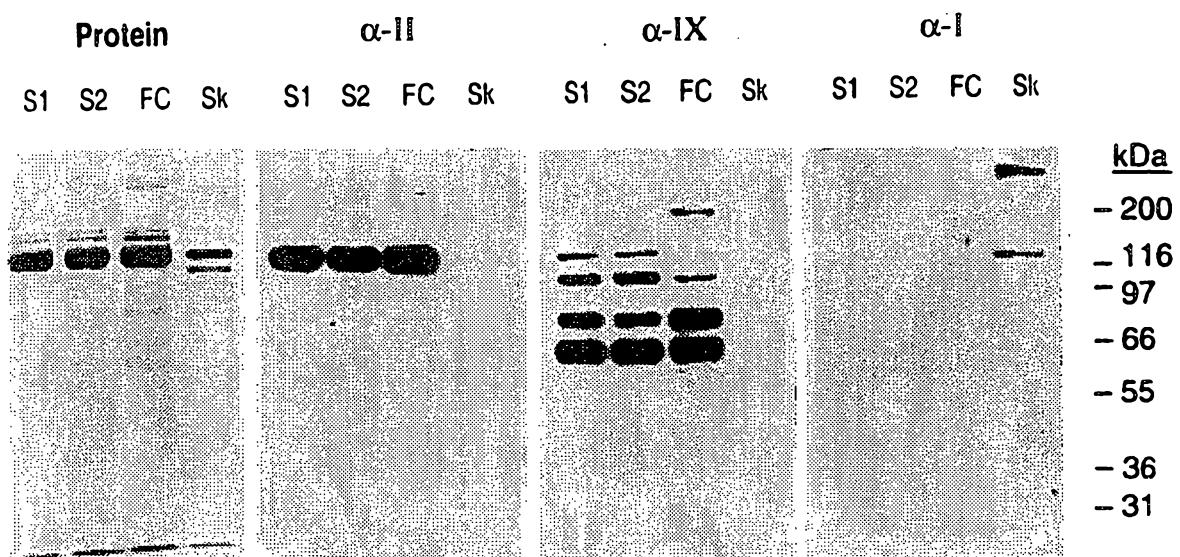


FIG. 8A

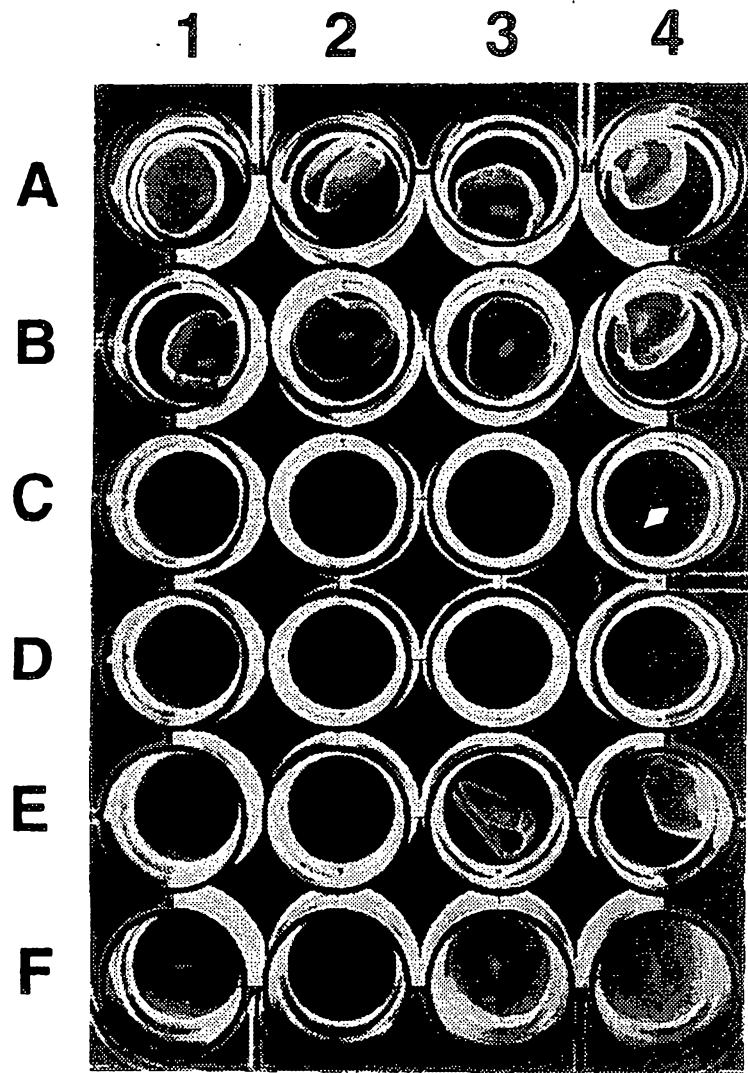


FIG. 8B

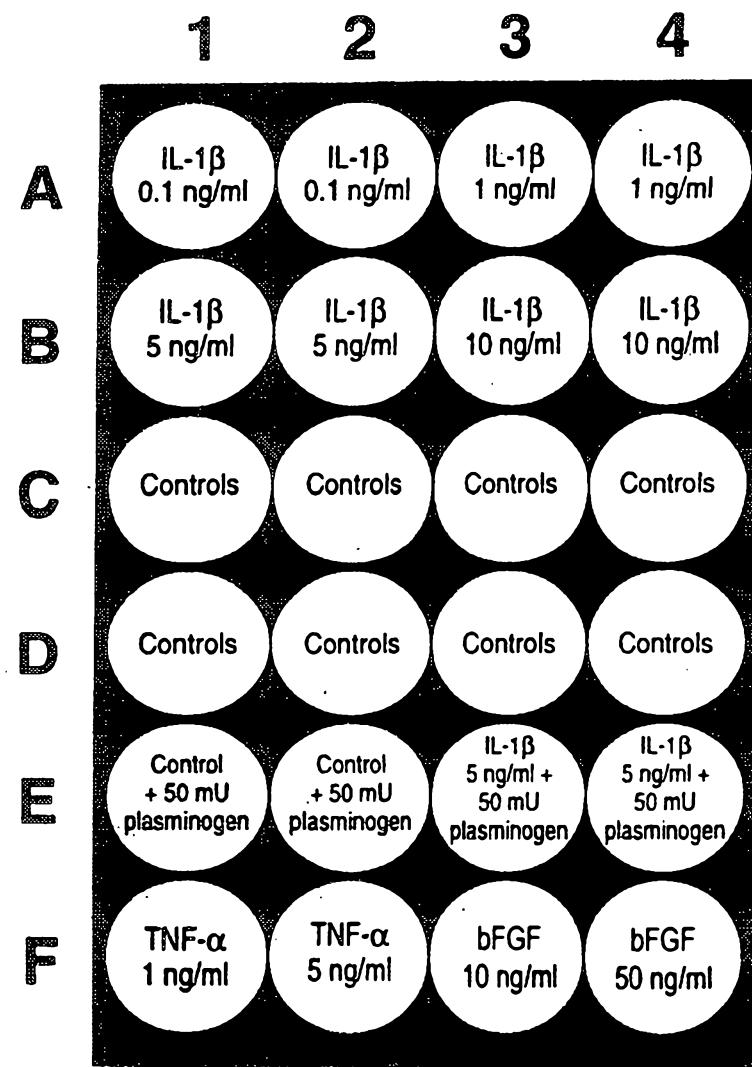


FIG. 9A

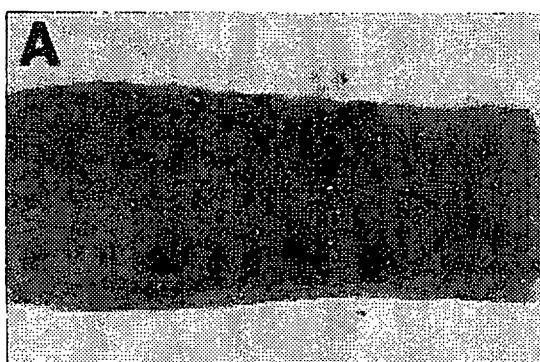


FIG. 9B

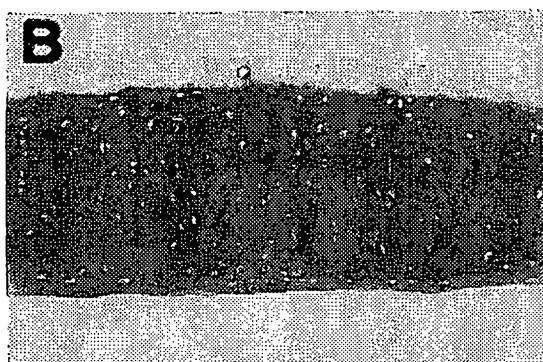


FIG. 9C

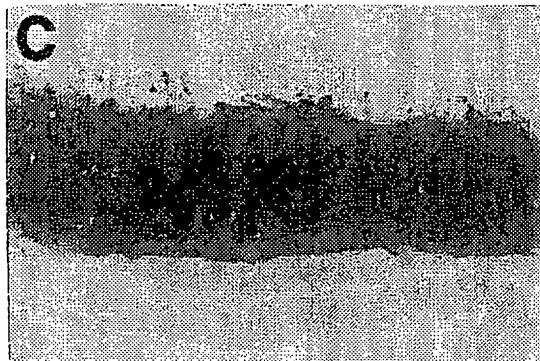


FIG. 9D

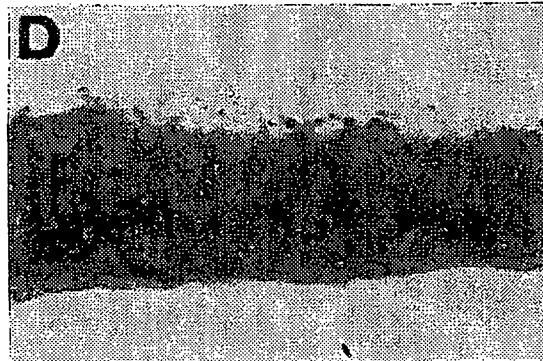


FIG. 10

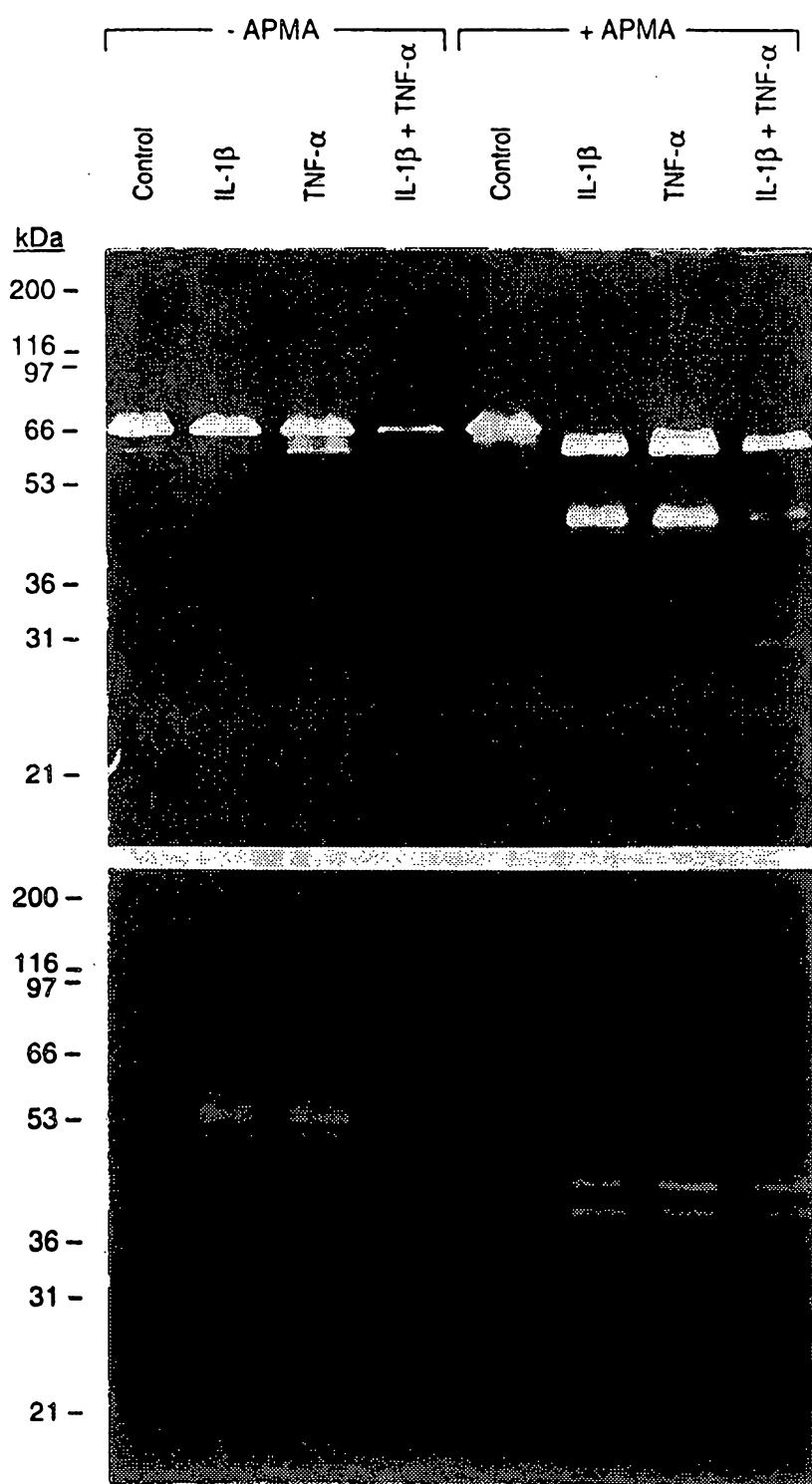


FIG. 11A



FIG. 11B

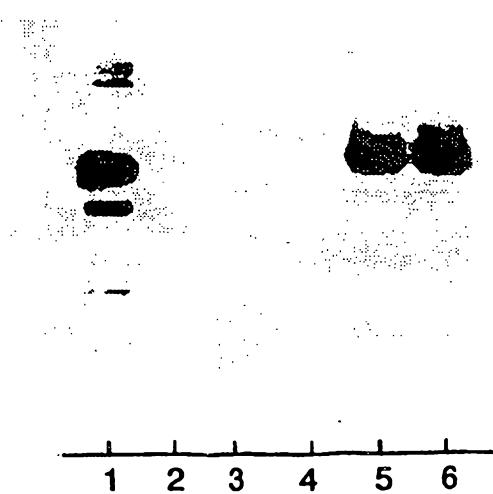


FIG. 12A

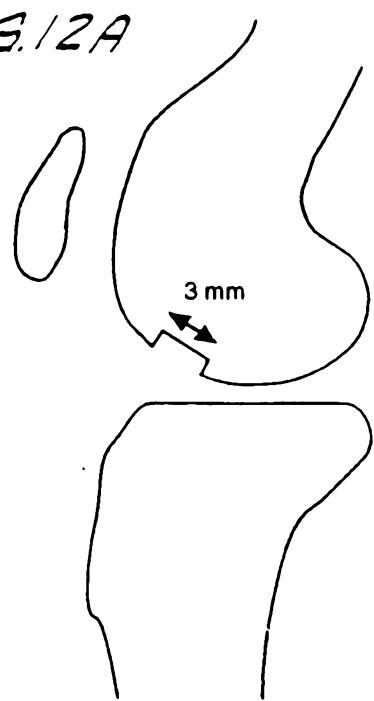


FIG. 12B

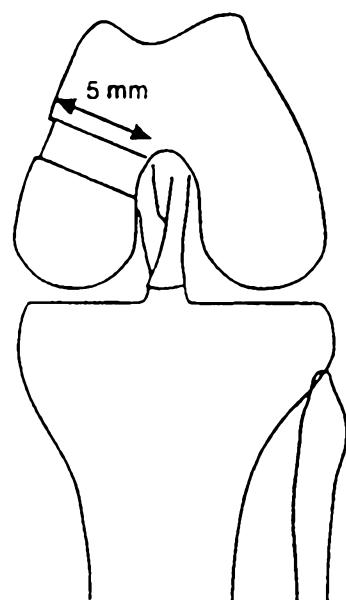


FIG. 12C

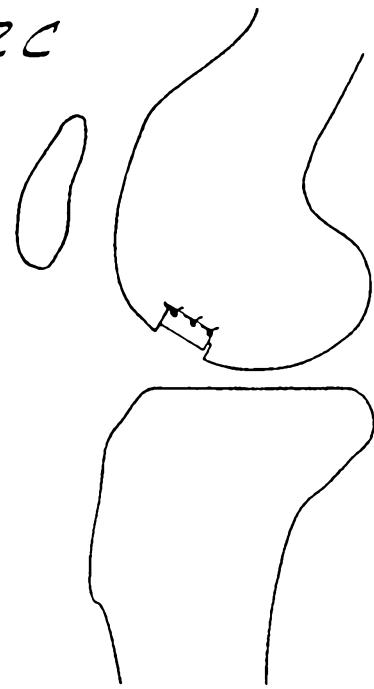


FIG. 12D

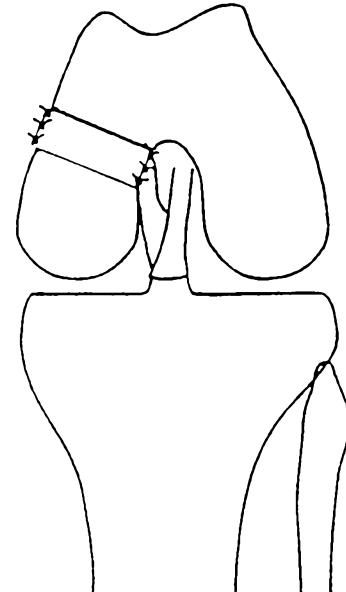


FIG.13A



FIG.13B



FIG. 14A

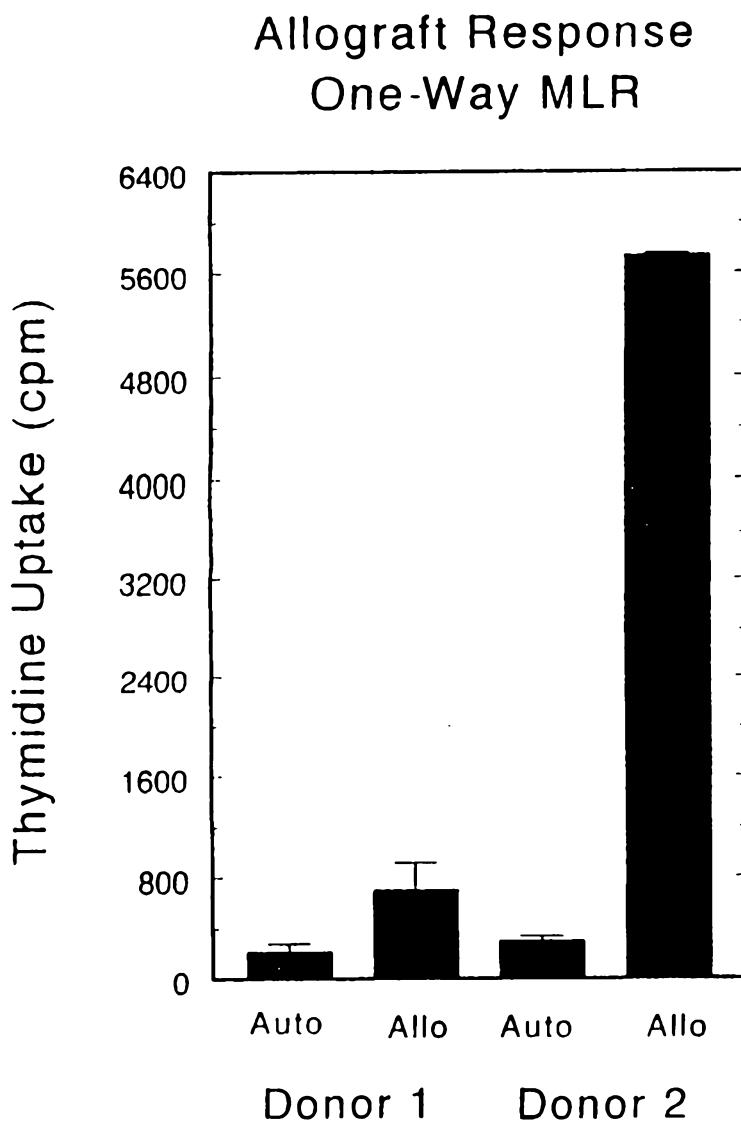


FIG. 14B

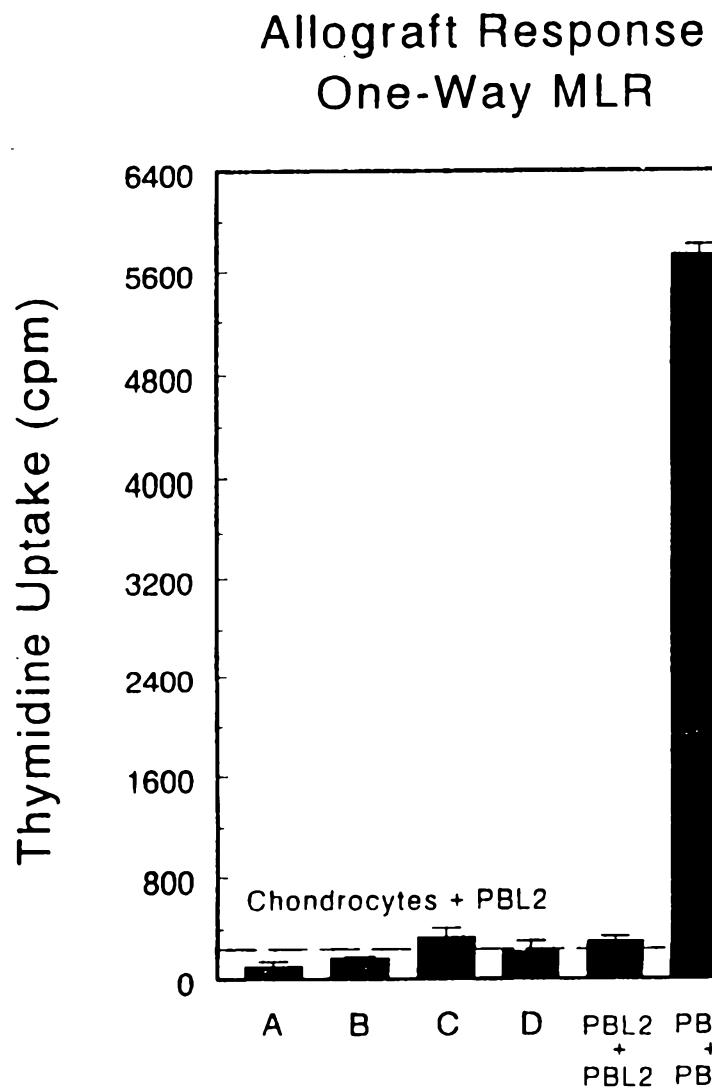


FIG. 15

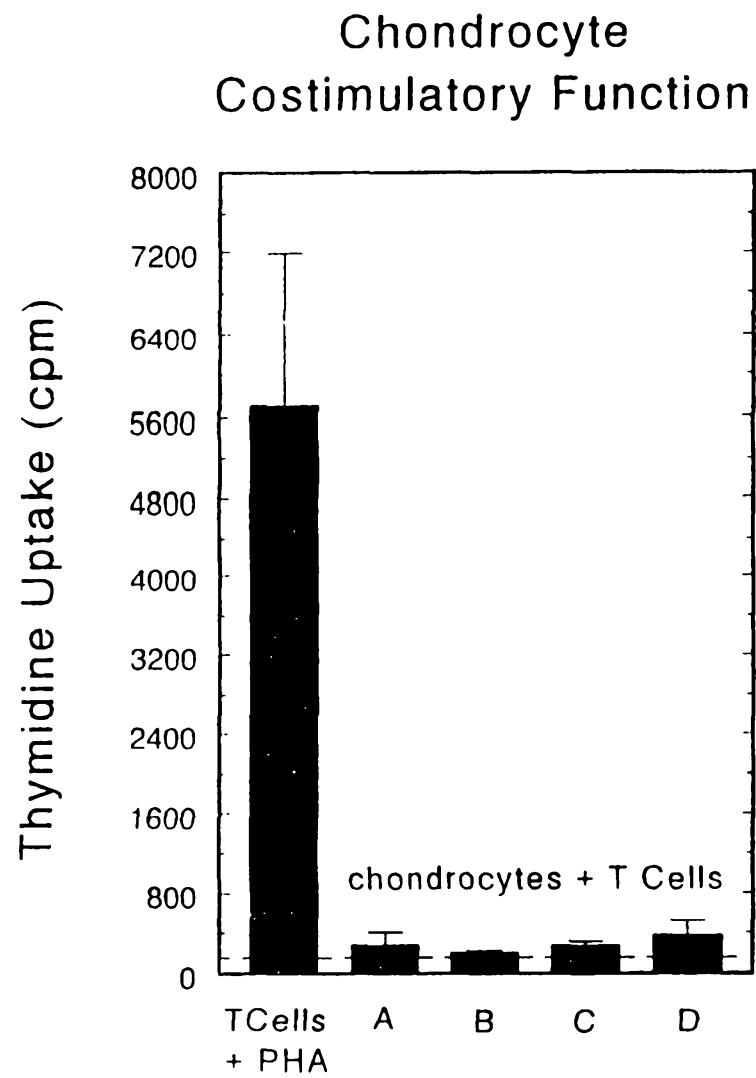


FIG. 16

Chondrocyte Overlay Increases
Neocartilage S-GAG Content

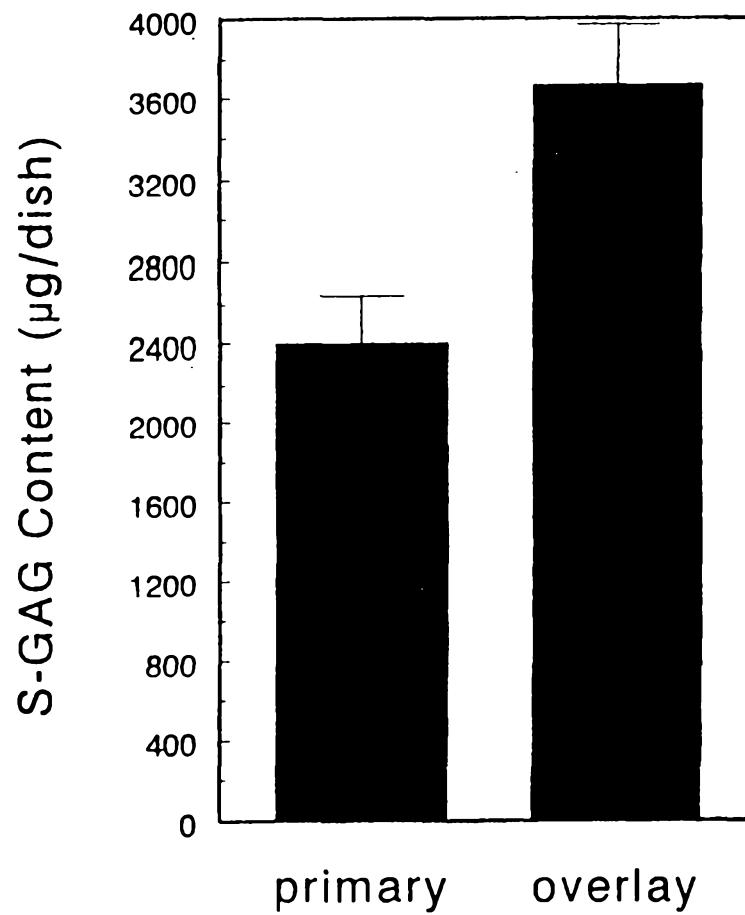


FIG. 17A

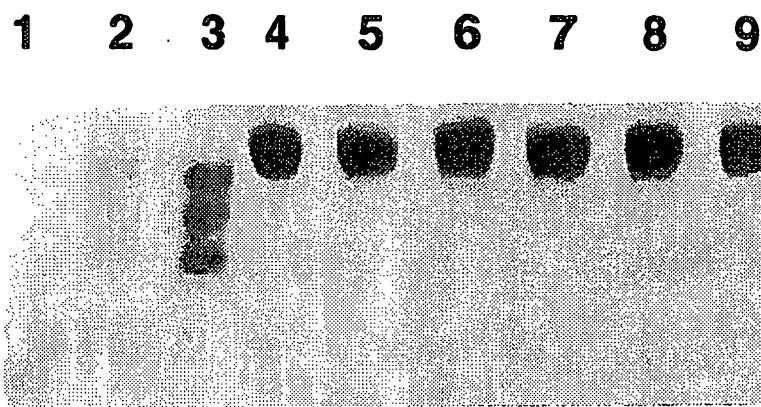


FIG. 17B

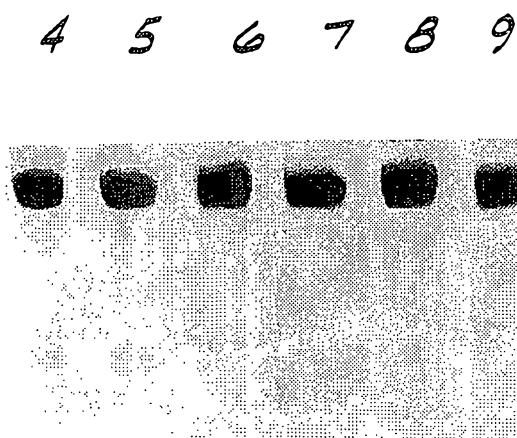


FIG. 18A

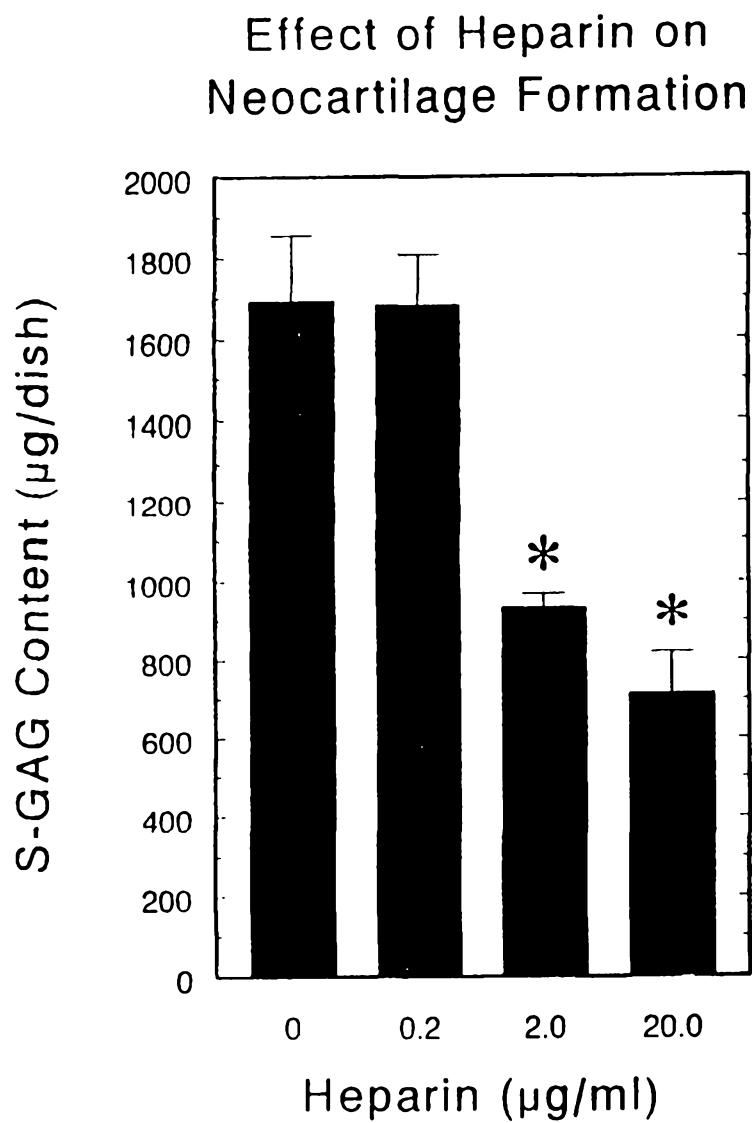


FIG. 18B

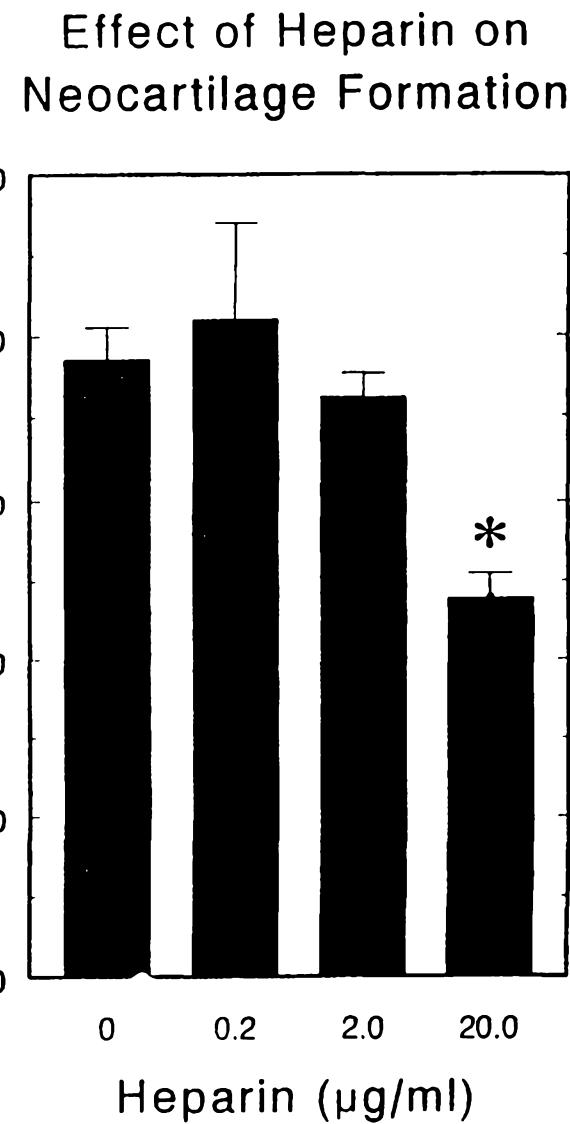


FIG. 19

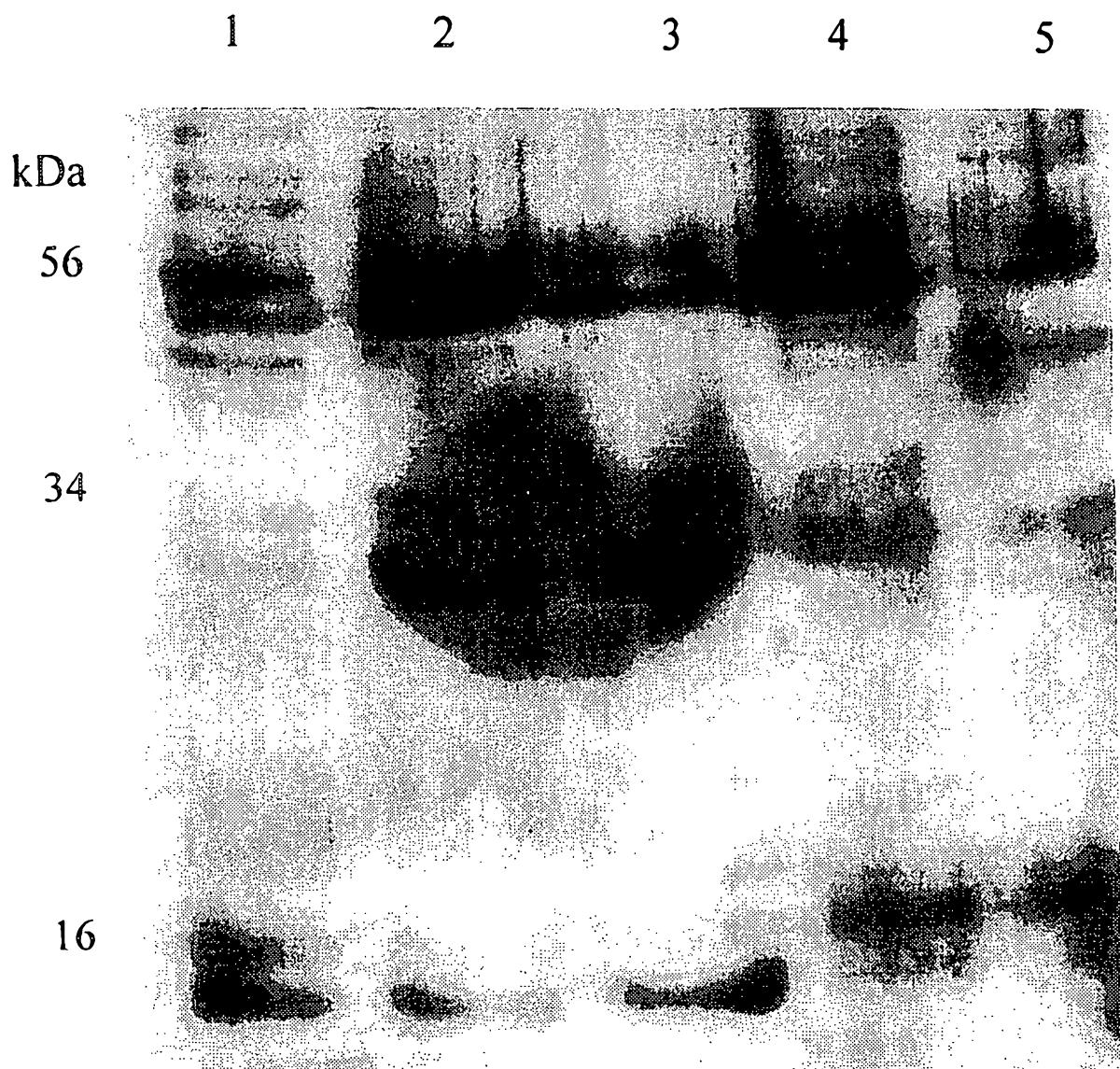


FIG. 20A

FATTY ACID COMPOSITION OF HUMAN FETAL ARTICULAR CHONDROCYTE PHOSPHOLIPIDS

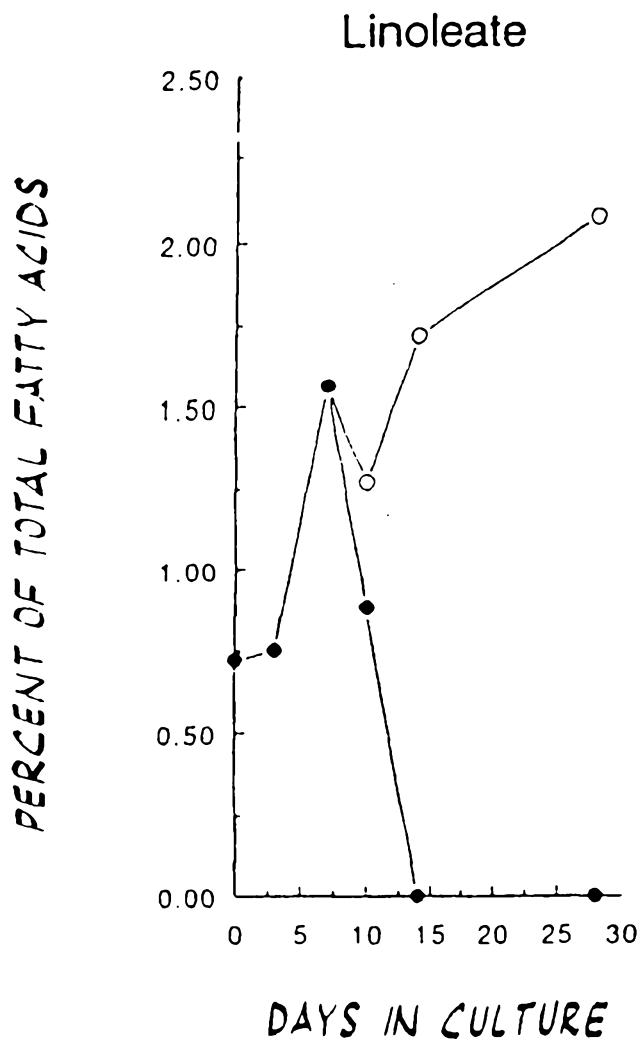


FIG. 20B

FATTY ACID COMPOSITION OF HUMAN FETAL ARTICULAR CHONDROCYTE PHOSPHOLIPIDS

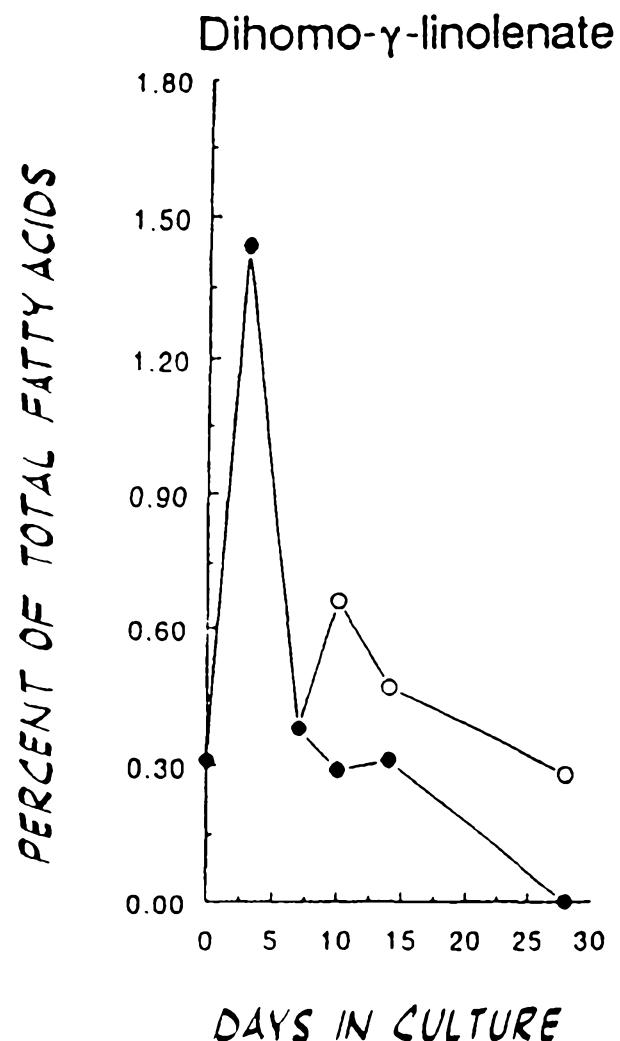


FIG. 20C

FATTY ACID COMPOSITION OF HUMAN FETAL ARTICULAR CHONDROCYTE PHOSPHOLIPIDS

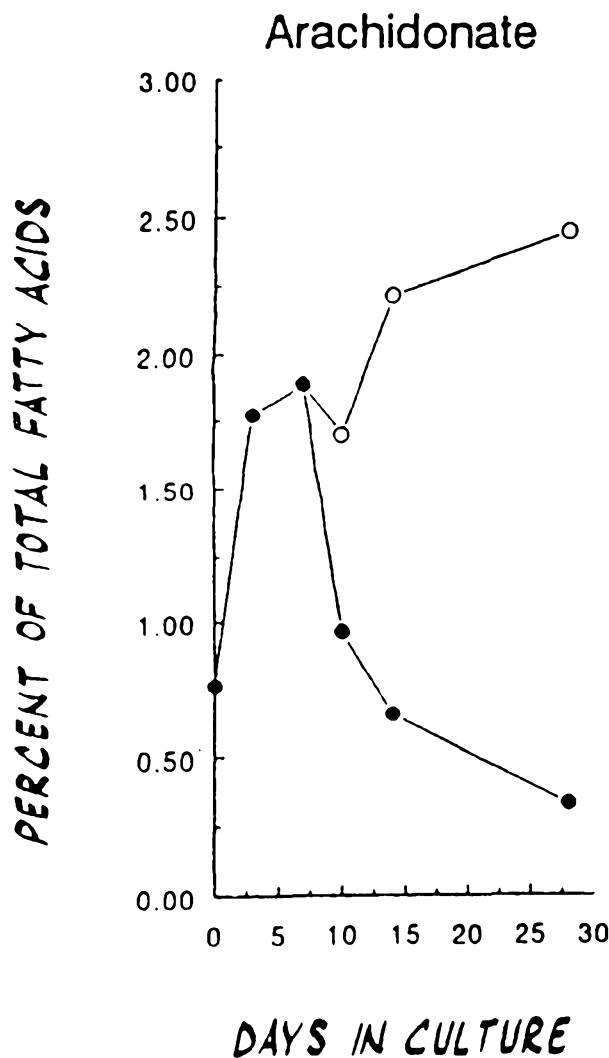


FIG. 20D

FATTY ACID COMPOSITION OF HUMAN FETAL ARTICULAR CHONDROCYTE PHOSPHOLIPIDS

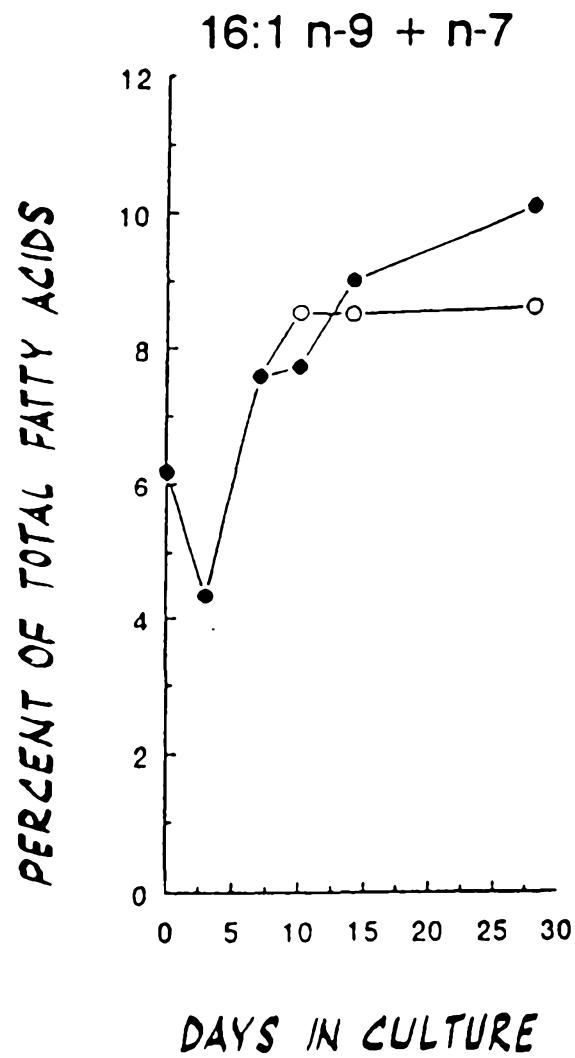
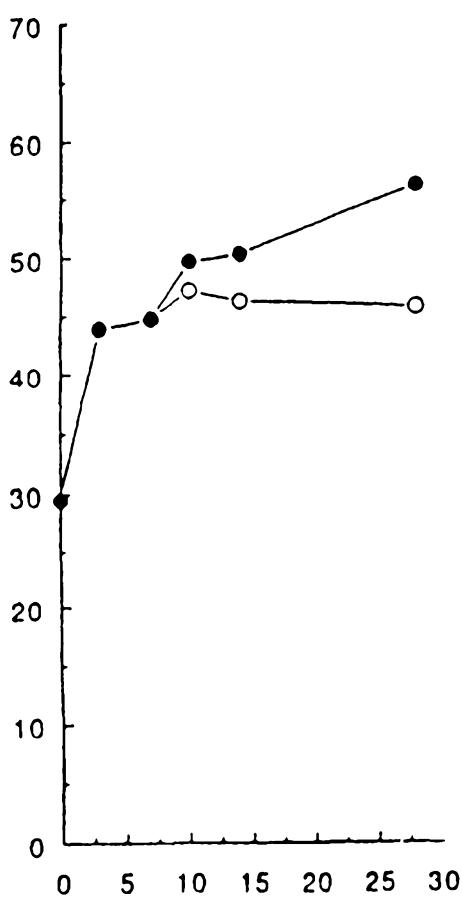


FIG. 20E

FATTY ACID COMPOSITION OF HUMAN FETAL ARTICULAR CHONDROCYTE PHOSPHOLIPIDS

18:1 n-9 + n-7

PERCENT OF TOTAL FATTY ACIDS



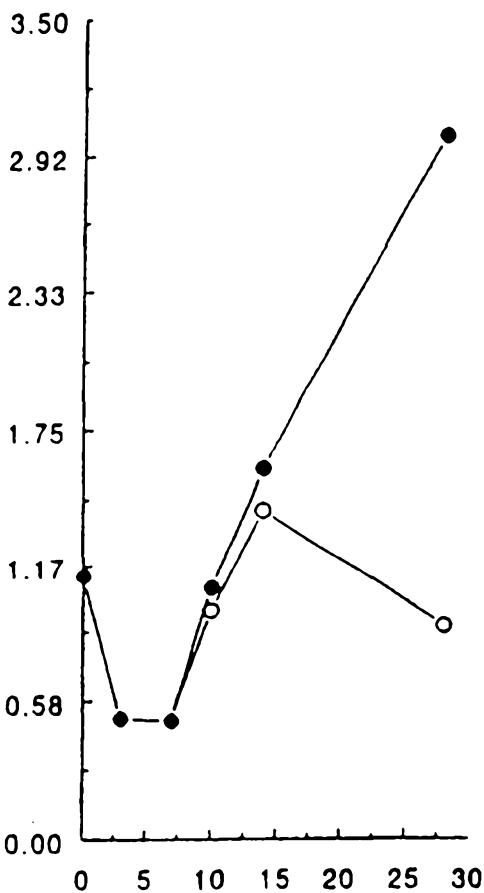
SUBSTITUTE SHEET (RULE 26)

FIG. 20F

FATTY ACID COMPOSITION OF HUMAN FETAL ARTICULAR CHONDROCYTE PHOSPHOLIPIDS

Mead

PERCENT OF TOTAL FATTY ACIDS



22 / 25

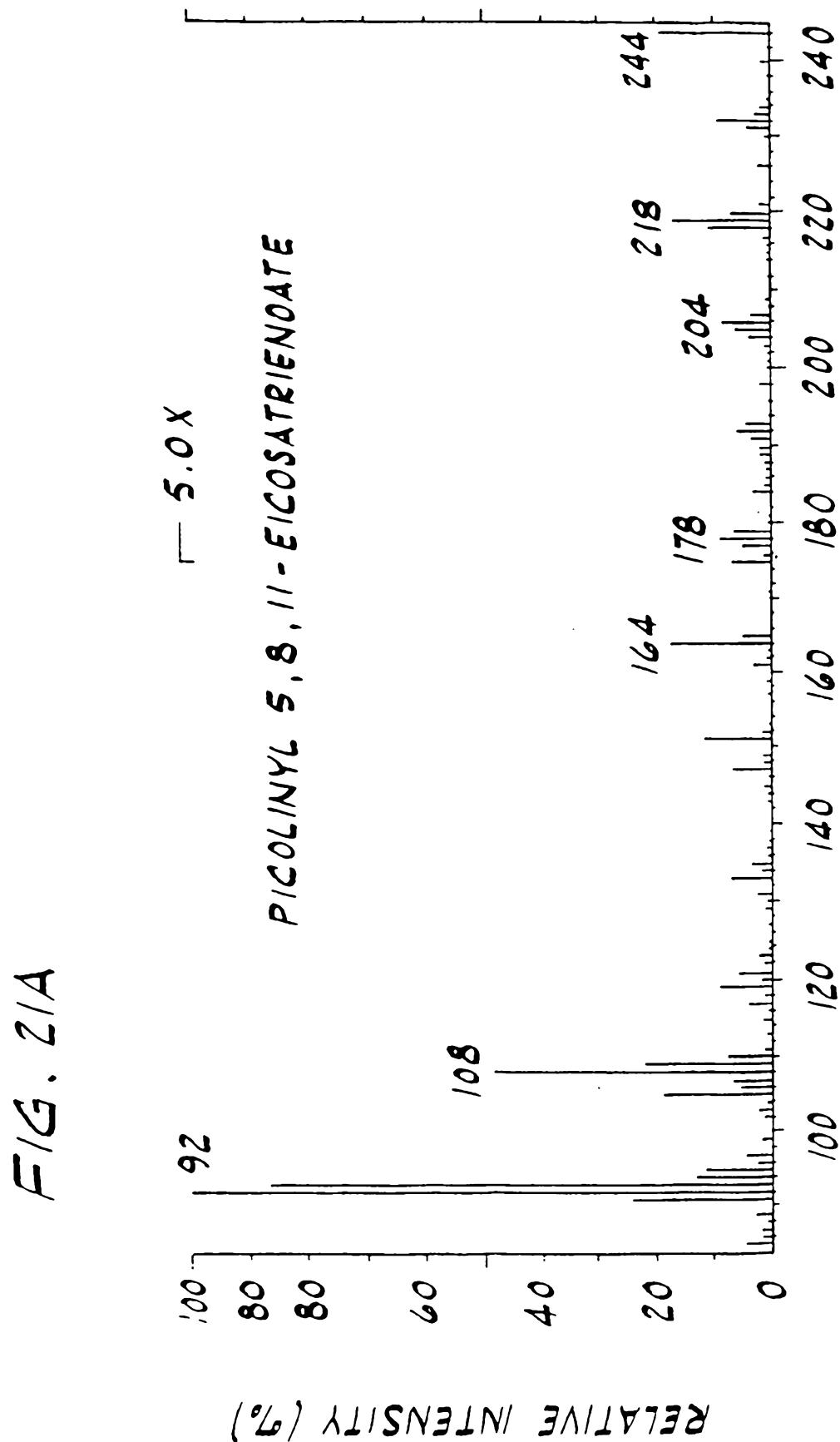
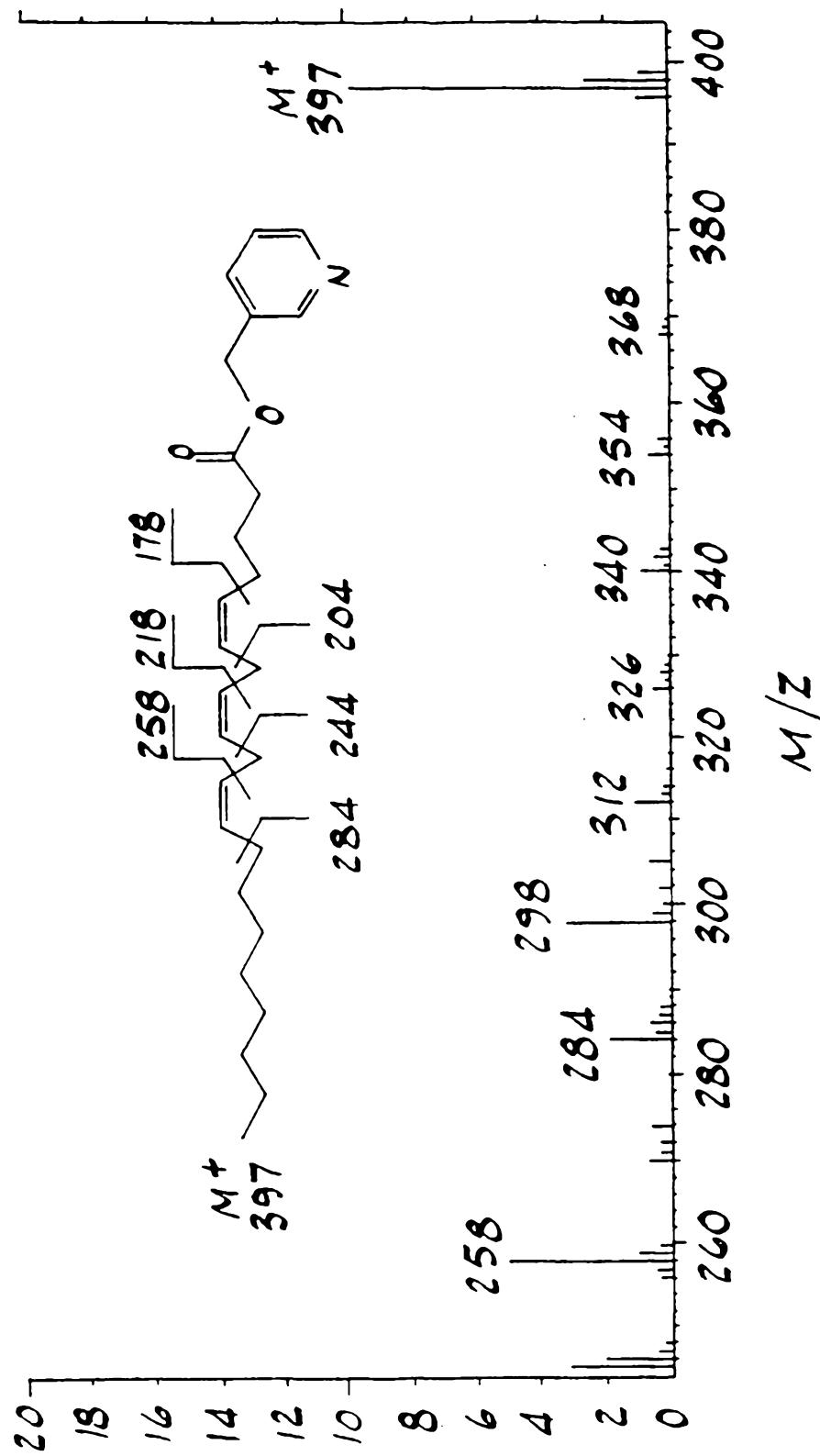


FIG. 21B



RELATIVE INTENSITY (%)

FIG. 22A

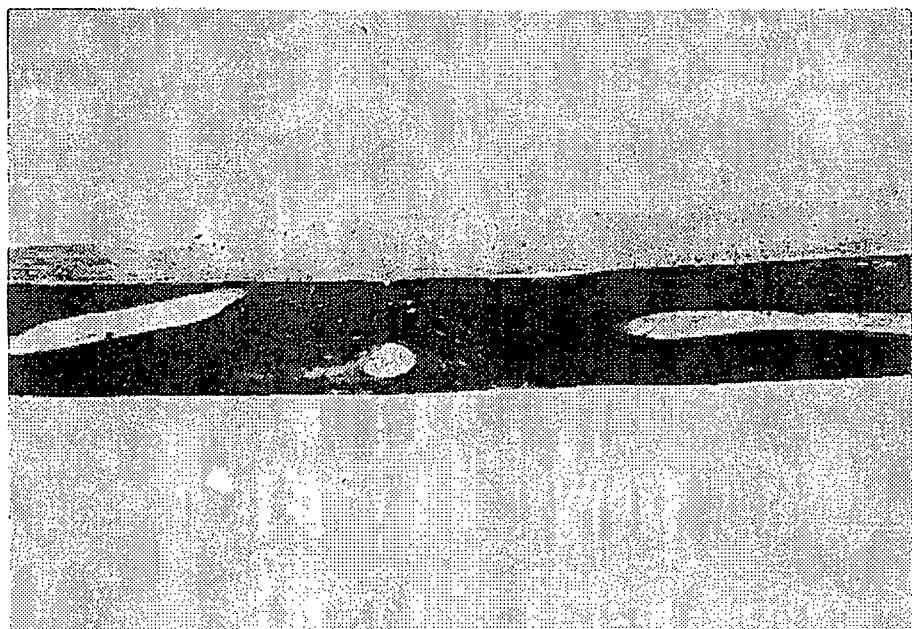


FIG. 22B

