US 20060213519A1

(19) United States

(12) Patent Application Publication (10) Pub. No.: US 2006/0213519 A1

Schmidt et al. (43) Pub. Date: Sep. 28, 2006

(54) CONTROL OF RESPIRATORY OXYGEN DELIVERY

(75) Inventors: **Matthew F. Schmidt**, Lino Lakes, MN (US); **John S. Buan**, Maple Grove, MN (US); **Catherine A. Nordman**, St. Paul, MN (US)

Correspondence Address:
MUETING, RAASCH & GEBHARDT, P.A.
P.O. BOX 581415
MINNEAPOLIS, MN 55458 (US)

(73) Assignee: **Minnesota Innovative Technologies and Instruments**, Lino Lakes, MN

(21) Appl. No.: **11/441,525**

(22) Filed: **May 26, 2006**

Related U.S. Application Data

(63) Continuation of application No. 10/695,436, filed on Oct. 28, 2003, which is a continuation of application No. 10/370,799, filed on Feb. 20, 2003, which is a continuation of application No. 10/076,001, filed on Feb. 14, 2002, now Pat. No. 6,561,187, which is a continuation of application No. 09/463,614, filed on May 8, 2000, now Pat. No. 6,371,114, filed as 371 of international application No. PCT/US98/15490, filed on Jul. 24, 1998, which is a continuation-in-part of application No. 08/900,686, filed on Jul. 25, 1997, now Pat. No. 6,532,958.

(60) Provisional application No. 60/064,578, filed on Nov. 4, 1997.

Publication Classification

(51) **Int. Cl.**
A61M 16/00 (2006.01)
A62B 7/00 (2006.01)

(52) **U.S. Cl.** **128/204.23**

(57) **ABSTRACT**

Methods and systems for supplying respiratory oxygen to users when the users are inhaling are disclosed. The methods and systems may rely on delivery devices that are selectively placed in fluid communication with either a respiration sensor or a source of oxygen. The methods and systems may actively monitor for exhalations, as well as monitor for oxygen in the oxygen source. The respiration sensor may preferably be a flow sensor.

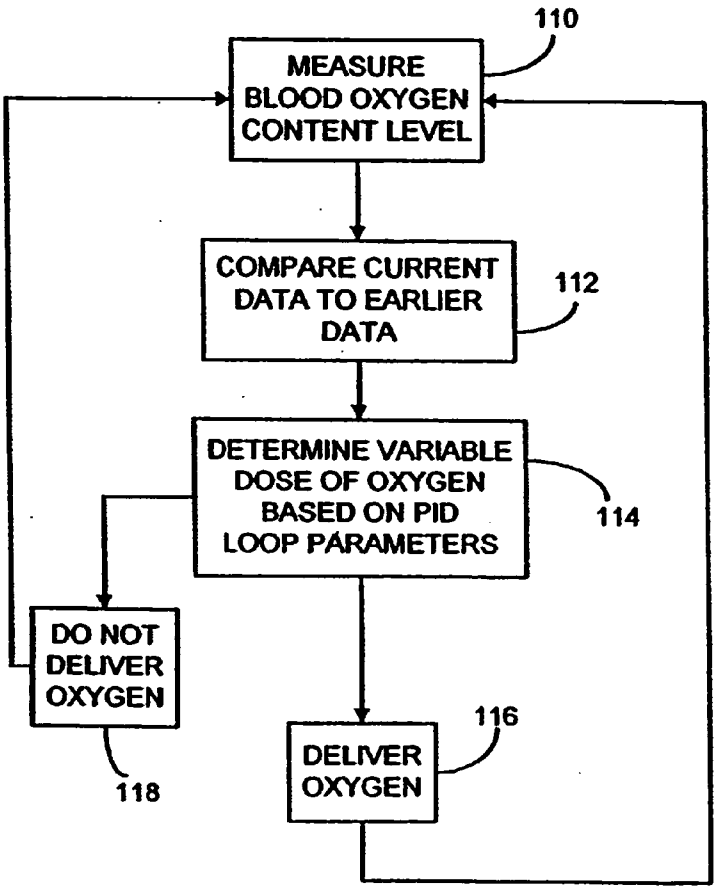


FIG. 1

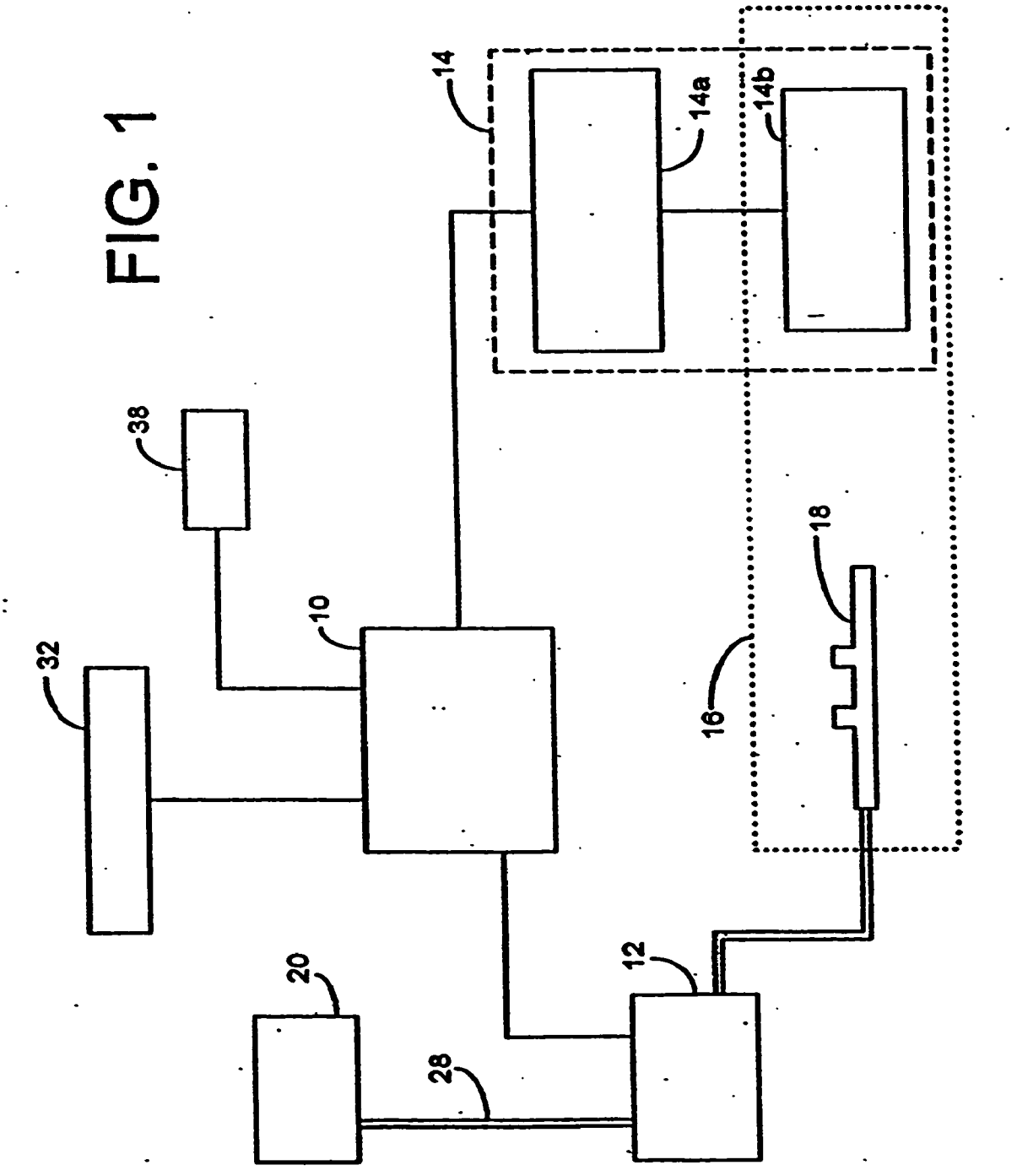
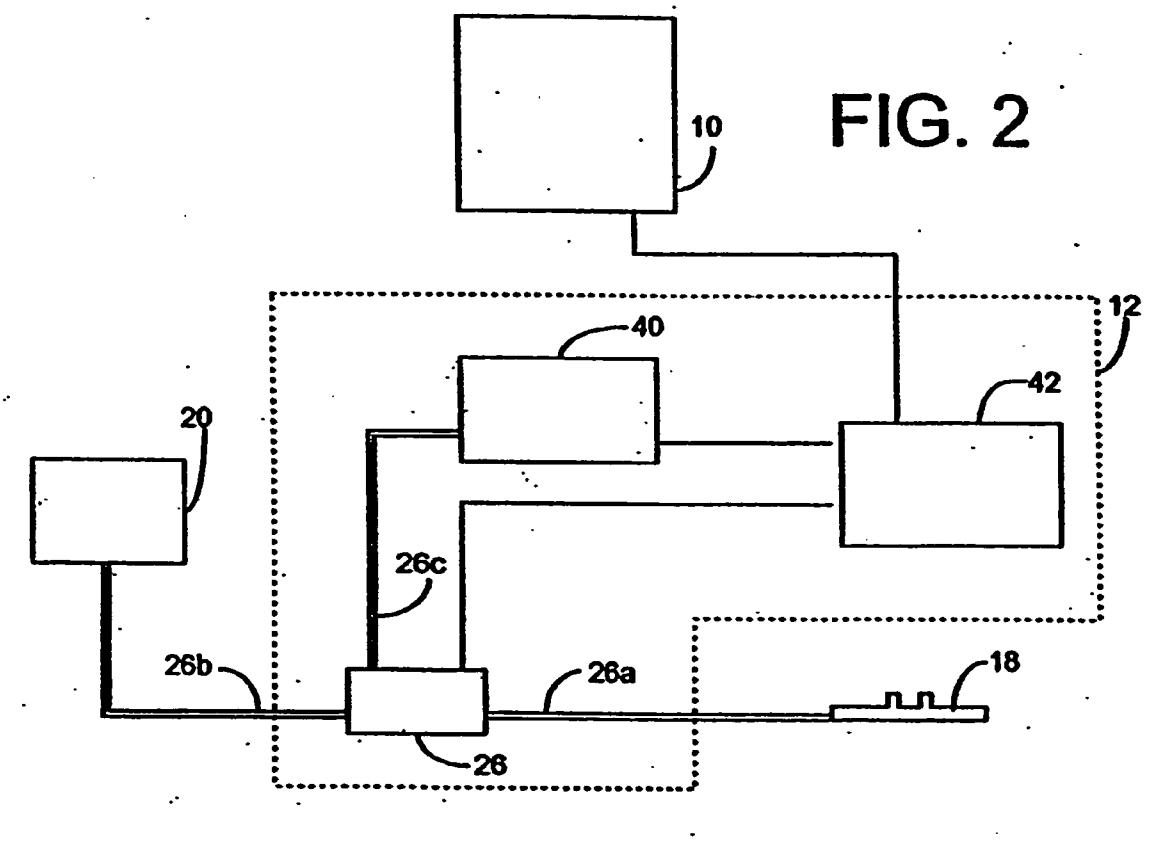


FIG. 2



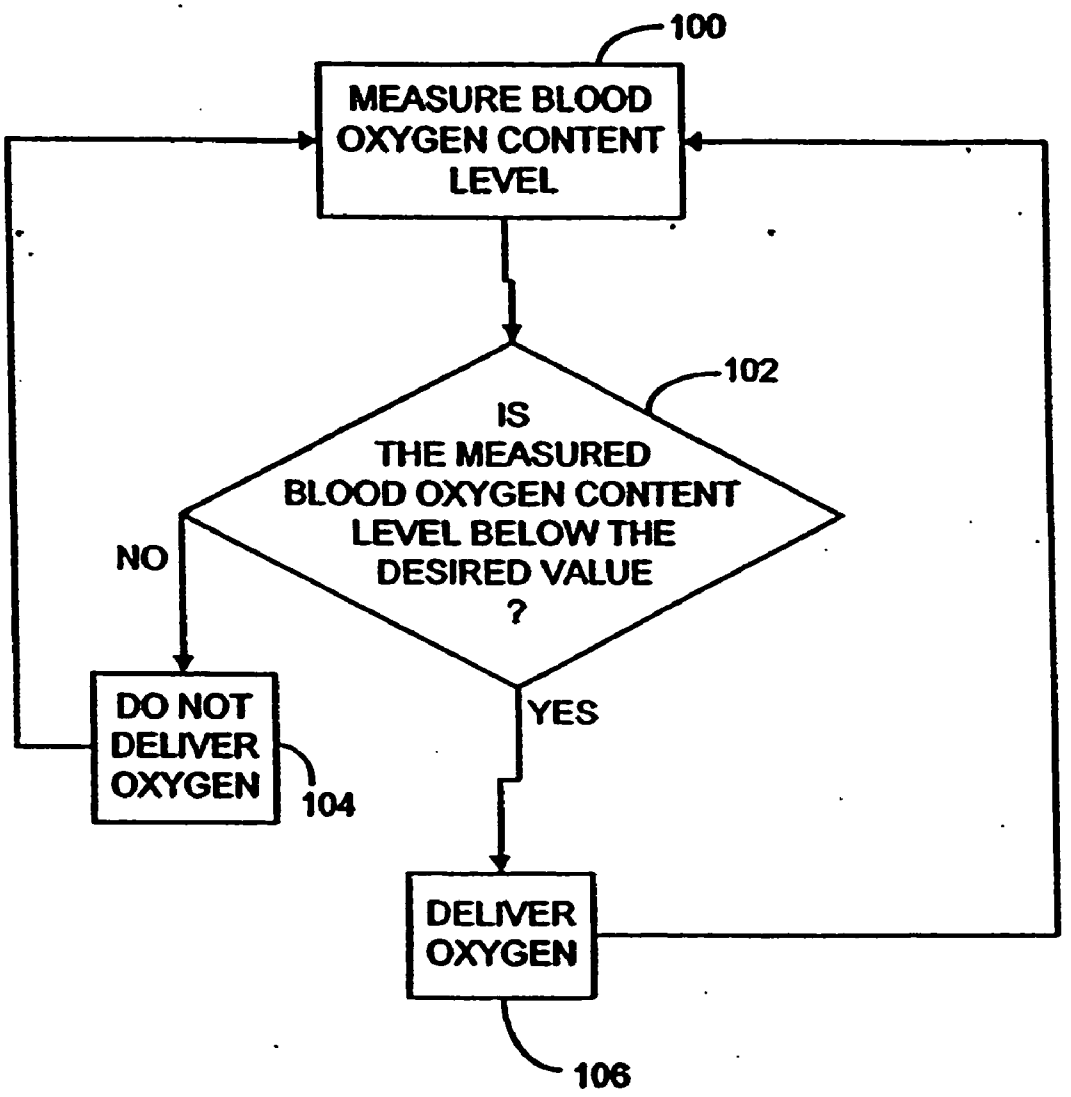

100
MEASURE BLOOD OXYGEN CONTENT LEVEL
102
IS THE MEASURED BLOOD OXYGEN CONTENT LEVEL BELOW THE DESIRED VALUE ?
NO
YES
DO NOT DELIVER OXYGEN
104
DELIVER OXYGEN
106

FIG. 3a

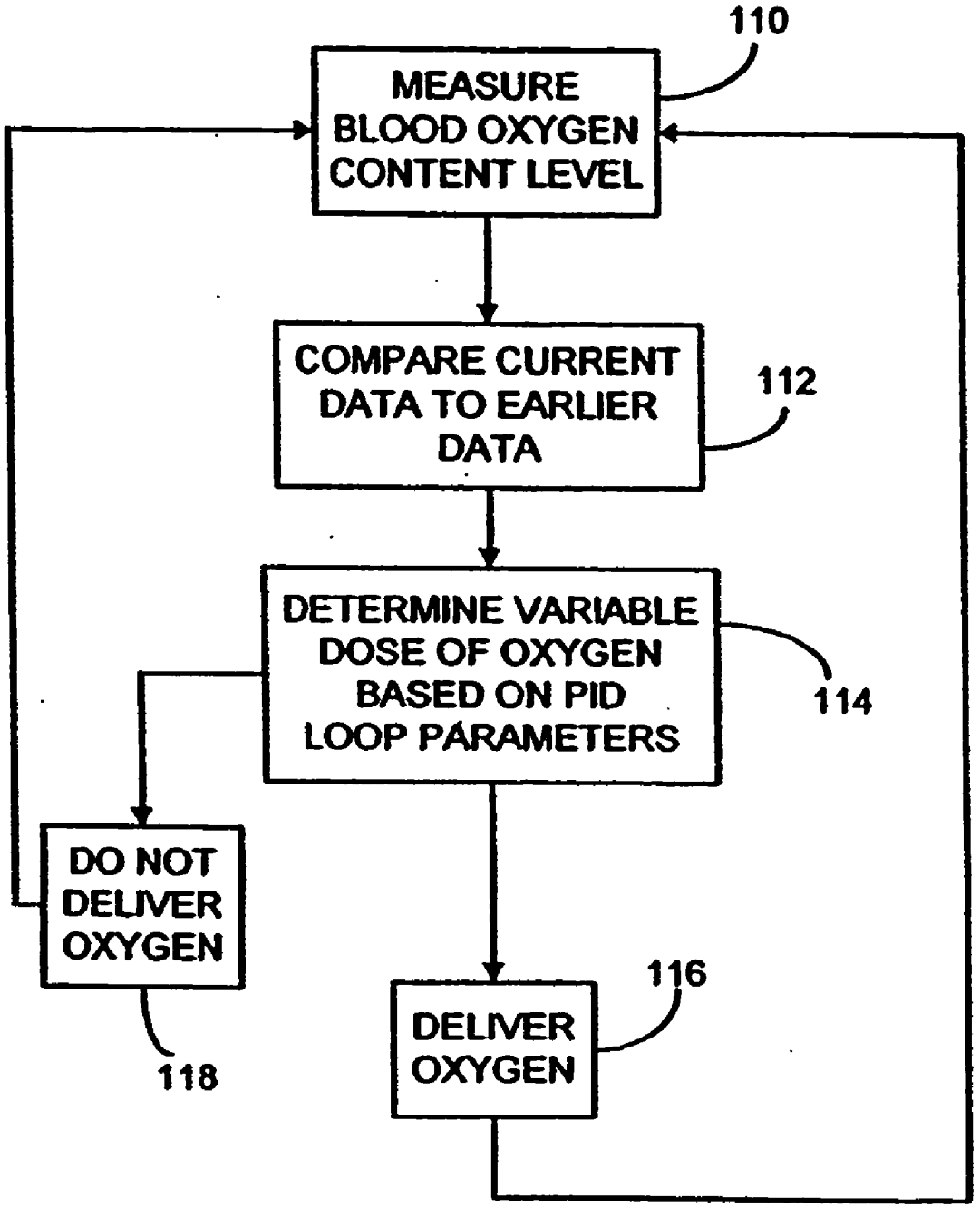

110
MEASURE BLOOD OXYGEN CONTENT LEVEL
COMPARE CURRENT DATA TO EARLIER DATA
112
DETERMINE VARIABLE DOSE OF OXYGEN BASED ON PID LOOP PARAMETERS
114
DO NOT DELIVER OXYGEN
118
116
DELIVER OXYGEN

FIG. 3b

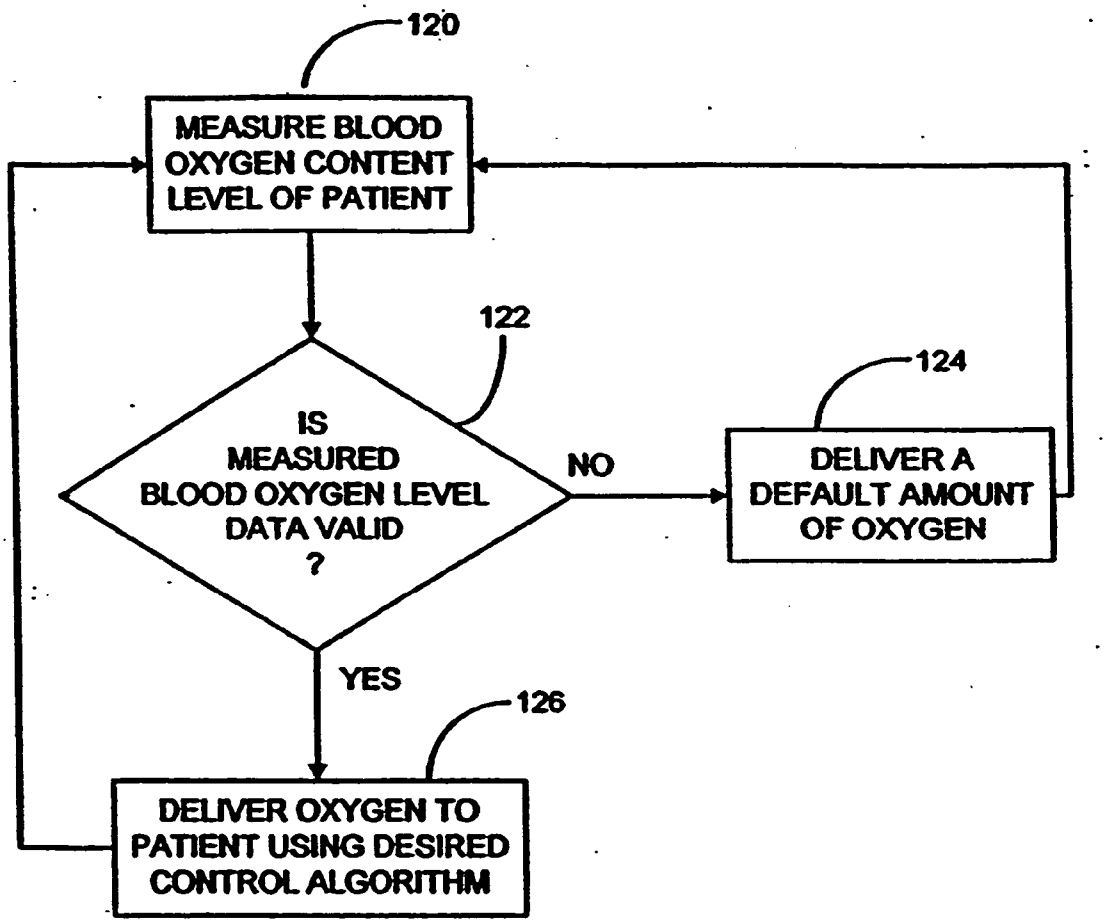

120
MEASURE BLOOD OXYGEN CONTENT LEVEL OF PATIENT
122
IS MEASURED BLOOD OXYGEN LEVEL DATA VALID ?
NO
124
DELIVER A DEFAULT AMOUNT OF OXYGEN
YES
126
DELIVER OXYGEN TO PATIENT USING DESIRED CONTROL ALGORITHM

FIG. 4

CONTROL OF RESPIRATORY OXYGEN DELIVERY

RELATED APPLICATIONS

[0001] This is a continuation of U.S. patent application Ser. No. 10/695,436, filed 28 Oct. 2003, which is a continuation of U.S. patent application Ser. No. 10/370,799, filed 20 Feb. 2003, which is a continuation of U.S. patent application Ser. No. 10/076,001, filed 14 Feb. 2002, (issued as U.S. Pat. No. 6,561,187), which is a continuation of U.S. patent application Ser. No. 09/463,614, filed 25 Jan. 2000 (with a 35 U.S.C. §371 date of May 8, 2000, now issued as U.S. Pat. No. 6,371,114), which is a U.S. National Stage Application of PCT/US98/15490, filed 24 Jul. 1998, which claims priority to U.S. Provisional Patent Application Ser. No. 60/064,578, filed 4 Nov. 1997 and which also claims priority to (and is a continuation-in-part of) U.S. patent application Ser. No. 08/900,686 filed 25 Jul. 1997, (issued as U.S. Pat. No. 6,532,958). All of the above-identified patent applications are incorporated herein by reference in their respective entireties

FIELD OF THE INVENTION

[0002] The present invention relates to the field of respiratory oxygen supply systems and methods. More particularly, the present invention provides demand delivery methods and systems that supply respiratory oxygen when the patient is inhaling.

BACKGROUND

[0003] Respiratory oxygen is delivered to patients in both sub-critical care situations in which oxygen is provided as a supplement to room air that may be inhaled by the patients (often referred to as "supplemental" oxygen delivery) and in critical care situations in which the gases (particularly oxygen) inspired by patients are closely controlled, possibly in connection with blood gas measurements.

[0004] Continuous oxygen delivery in sub-critical and critical care is, however, wasteful because oxygen is only needed by patients when they are inhaling and the oxygen delivered at other times is wasted. In supplemental oxygen delivery, the most significant financial cost associated with this waste is found in the increased service visits required by the oxygen provider to replenish the patient's oxygen supply, because the actual cost of the oxygen is only a small fraction of the total cost of the therapy. In critical care environments, the capacity of the oxygen delivery system must be increased to account for the oxygen delivered when the patient is exhaling.

[0005] One approach to conserving the oxygen delivered to patients is typically referred to as "demand delivery." The demand delivery systems respond to a patient's inspiratory effort by attempting to deliver oxygen during the period of inhalation, rather than allow the oxygen to flow to the patient continuously. There are many ways in which this basic concept has been implemented.

[0006] A variety of respiration detection systems have been developed in connection with demand delivery systems. Examples of some respiration detectors include a chest belt worn by the patient that generates an electrical signal to trigger the opening of the oxygen supply valve; a hand-activated breathing device attached to a portable gas bottle via a supply hose in which users dispense the oxygen by pushing a button while holding the device next to their mouth; a mechanical chest strap/valve that functions as both an inhalation sensor and delivery device in an oxygen conserving system; and an all-pneumatic, fluidically-controlled device.

[0007] Other demand delivery systems use pressure sensors in the oxygen line to monitor line pressure at the nostrils. A small negative pressure, indicative of the onset of inhalation, is often relied on to trigger the release of oxygen. This type of detection scheme has become a standard method of demand delivery and is employed by most systems currently in use.

[0008] Yet another approach employs flow sensors to monitor patient respiration. In many of these demand delivery systems, the flow sensors are located in-line with the source of oxygen such that, in addition to monitoring patient respiration, the flow sensors also monitor the amount of oxygen passing through them during the oxygen delivery portion of the cycle. It is, however, difficult (if not impossible) to accomplish both of those functions with a single flow sensor because the flow rates that need to be sensed differ by orders of magnitude. For example, when measured using a nasal cannula, patient respiration may result in flow rates at the flow sensor of about 1 cubic centimeters per minute (cc/min) or less, while the flow rate of oxygen delivered to the patient can be up to about 15 liters per minute (1/min) or more. One significant problem is in sensing inhalation or exhalation simultaneously with the delivery of oxygen in these situations. Examples of this approach are found in U.S. Pat. No. 4,823,788 (Smith et al.) and U.S. Pat. No. 5,558,086 (Smith et al.).

[0009] In addition to the above-listed problems, even if the flow sensor has a dynamic range capable of sensing respiration and delivery oxygen, the systems do not allow for correction in the "drift" often associated with such sensors. In other words, over time the accuracy of the sensor may be impaired because of dynamic changes in the flow sensor during use. Because the flow sensors are always in use, monitoring either oxygen flow or respiration, adjustments are difficult if not impossible to make to correct for voltage drift.

[0010] Another flow sensor-based demand delivery system is described in U.S. Pat. No. 5,074,299 (Dietz) in which a flow sensor is connected to one port of a nasal cannula while oxygen is delivered through the other port of the cannula. One disadvantage to this approach is that if one side of the patient's nasal cavity is blocked due to an upper respiratory infection or cold, the system will either be unable to effectively deliver oxygen or sense respiration (depending on which port of the cannula is located on the blocked side).

[0011] Even if the patient is not experiencing blockage, it may be difficult for the sensor to detect exhalation if the patient is breathing through his or her mouth. The nasal respiratory flow rate is significantly reduced in such patients, and if flow sensing is occurring only through one port in the cannula, it may be too low to be accurately detected. Another disadvantage is that the system requires a more expensive and obscure dual-line cannula.

[0012] Regardless of whether pressure or flow sensors are used to detect respiration, shallow respiration can make

respiration sensing in systems relying on pressure/flow sensors difficult or impossible because the flow volume and/or flow rate of gases associated with respiration deteriorate as the gases from inhalation or exhalation travel through the lines connecting the patient's respiratory system to the sensor. The flow volume/rate deterioration caused by the lines further reduces the flow volume/rate produced by a patient engaging in shallow respiration. As a result, the respiration sensor may be unable to detect respiration or may detect only a portion of the actual inhalation/exhalation events.

[0013] Another problem associated with patients experiencing rapid respiration rates is that some demand delivery systems include a time delay period to prevent sensing of the same inhalation period more than once. These systems operate on the assumption that each inhalation lasts for a predetermined minimum amount of time and the system is prevented from sensing inhalation within the delay period. Because the patient is, however, experiencing rapid respiration, the patient may actually inhale two or more times during the delay period. The effect of such a "lockout" feature is that the patient will receive oxygen during only a fraction of their inhalation events. In addition, if the respirations are rapid and the system delivers oxygen too slowly, the patient may already be exhaling by the time the system begins to deliver oxygen.

SUMMARY OF THE INVENTION

[0014] The present invention provides respiratory oxygen supply methods and systems. In some aspects, the systems/methods rely on respiration sensors sensing variations in patient respiration to determine when a patient is inhaling and allow for the determination of an inhalation event after exhalation has been determined. In other aspects, the respiration sensors may be advantageously used to detect the presence of oxygen from the oxygen supply. In still other aspects, when the present invention uses a flow sensor as a respiration sensor, the system may automatically correct for variations in the signals provided by the flow sensor using a zero-flow offset signal, thereby improving the accuracy of the system.

[0015] In one aspect, the present invention provides a method of delivering respiratory oxygen to a patient by providing an oxygen delivery system including an oxygen delivery device, a respiration sensor, and an oxygen source; placing the delivery device in fluid communication with the respiration sensor and monitoring variations in respiration with the respiration sensor to determine when the patient is inhaling; placing the oxygen source in fluid communication with the delivery device; delivering oxygen to the delivery device from the oxygen source when the patient is inhaling; removing the respiration sensor from fluid communication with the delivery device when delivering oxygen to the delivery device from the oxygen source; placing the respiration sensor in fluid communication with the delivery device after delivering oxygen to the delivery device from the oxygen source; monitoring variations in respiration with the respiration sensor after delivering oxygen to the delivery device from the oxygen source to determine when the patient is exhaling; and resuming the monitoring of variations in respiration with the respiration sensor to determine that the patient is inhaling after determining that the patient has exhaled.

[0016] In another aspect, the present invention provides a method of delivering respiratory oxygen to a patient by providing an oxygen delivery system including an oxygen delivery device, a respiration sensor, and an oxygen source; placing the delivery device in fluid communication with the respiration sensor and monitoring variations in respiration with the respiration sensor to determine when the patient is inhaling; placing the oxygen source in fluid communication with the delivery device; delivering oxygen to the delivery device from the oxygen source when the patient is inhaling; removing the respiration sensor from fluid communication with the delivery device when delivering oxygen to the delivery device from the oxygen source; placing the respiration sensor in fluid communication with the delivery device after delivering oxygen to the delivery device from the oxygen source; and monitoring the respiration sensor to detect oxygen in the oxygen source.

[0017] In another aspect, the present invention provides a method of delivering respiratory oxygen to a patient by providing an oxygen delivery system including an oxygen delivery device, a flow sensor, and an oxygen source; placing the delivery device in fluid communication with the flow sensor and monitoring variations in respiration with the flow sensor to determine when the patient is inhaling; placing the oxygen source in fluid communication with the delivery device; delivering oxygen to the delivery device from the oxygen source when the patient is inhaling; removing the respiration sensor from fluid communication with the delivery device when delivering oxygen to the delivery device from the oxygen source; placing the flow sensor in fluid communication with the delivery device after delivering oxygen to the delivery device from the oxygen source; monitoring a zero-flow offset signal produced by the flow sensor when it is not in fluid communication with the delivery device; and compensating for drift in the zero-flow offset signal generated by the flow sensor based on the monitoring when the flow sensor is not in fluid communication with the delivery device.

[0018] In another aspect, the present invention provides a method of delivering respiratory oxygen to a patient by providing an oxygen delivery system including an oxygen delivery device, a bidirectional flow sensor vented to atmosphere, and an oxygen source; placing the delivery device in fluid communication with the flow sensor and monitoring variations in respiration with the flow sensor to determine when the patient is inhaling; placing the oxygen source in fluid communication with the delivery device; delivering oxygen to the delivery device from the oxygen source when the patient is inhaling; removing the flow sensor from fluid communication with the delivery device when delivering oxygen to the delivery device from the oxygen source; placing the flow sensor in fluid communication with the delivery device after delivering oxygen to the delivery device from the oxygen source; monitoring variations in respiration with the flow sensor when it is in fluid communication with the delivery device to determine when the patient is exhaling before resuming the monitoring of variations in respiration with the flow sensor to determine that the patient is inhaling; monitoring a zero-flow offset signal produced by the flow sensor when it is not in fluid communication with the delivery device; compensating for drift in the zero-flow offset signal generated by the flow sensor based on the monitoring when the flow sensor is not in fluid communication with the delivery device; and monitoring the

flow sensor to detect oxygen in the oxygen source when switching the delivery device from fluid communication with either of the oxygen source and the flow sensor.

[0019] In another aspect, the present invention provides a system for delivering respiratory oxygen to a patient including a delivery line adapted for connection to an oxygen delivery device located on a patient; a source line adapted for connection to an oxygen source; a respiration sensor; at least one valve in fluid communication with the delivery line, the source line and the respiration sensor; wherein the at least one valve places the delivery line in fluid communication with only one of the source line and the respiration sensor at any given time; means for monitoring the respiration sensor for variations in respiration of a patient; means for determining when the patient is inhaling and exhaling based on the monitoring of the respiration sensor; and means for preventing a determination that the patient is inhaling until after a determination that the patient has exhaled has been made.

[0020] In another aspect, the present invention provides a system for delivering respiratory oxygen to a patient including a delivery line adapted for connection to an oxygen delivery device located on a patient; a source line adapted for connection to an oxygen source; a respiration sensor; at least one valve in fluid communication with the delivery line, the source line and the respiration sensor; wherein the at least one valve places the delivery line in fluid communication with only one of the source line and the respiration sensor at any given time; means for monitoring the respiration sensor to detect oxygen in the source line.

[0021] As used in connection with the present invention, the terms "supplemental oxygen" and "supplemental respiratory oxygen" refer to oxygen delivered to patients in addition to the oxygen received by the patient through the inspiration of room or ambient air. Because room air contains some oxygen, the supplemental oxygen is provided in addition to the oxygen that would normally be inspired by the patient.

[0022] As used in connection with the present invention, the term "blood oxygen content" and "blood oxygen content level" will typically be used to refer to blood oxygen saturation as commonly measured by the percentage of oxygen-saturated hemoglobin (SpO_2) although it can also refer to any suitable measurement for determining the level of oxygenation in a patient's blood. For example, it will be understood that blood oxygen content can also be obtained based on data from a CO-oximeter. Furthermore, blood oxygen content, can also be obtained based on partial pressures of oxygen (PaO_2).

[0023] As used in connection with the present invention, the term "sub-acute care" refers to care provided to patients that is not intended to treat critical conditions. Typically, sub-acute care is provided to patients in residential settings. "Residential" preferably includes, e.g., homes and long-term care facilities (such as nursing homes). Sub-acute care also includes care delivered in ambulatory situations, i.e., when the patient is engaged in normal activities outside of his or her residence, such as shopping, attending concerts or other events, traveling to appointments with health care professionals, etc.

[0024] As used in connection with the present invention, the terms "continuous" and "continuously" (when referring to the measuring of blood oxygen content levels) mean that the blood oxygen content level of the patient will be measured without cessation or at intervals (fixed or variable) that are sufficiently small to provide the advantages of the invention.

[0025] These and other features and advantages of the present invention will be apparent upon review of the detailed description of the invention and accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

[0026] **FIG. 1** is a block diagram of one system according to the present invention.

[0027] **FIG. 2** is a block diagram of one demand delivery module for use in a system such as that depicted in **FIG. 1**.

[0028] **FIG. 3*a*** is a flow diagram of one method according to the present invention.

[0029] **FIG. 3*b*** is a flow diagram of another method according to the present invention.

[0030] **FIG. 4** is a flow diagram of one method of delivering supplemental oxygen based on whether the measured blood oxygen content data is valid or invalid.

DETAILED DESCRIPTION OF ILLUSTRATIVE EMBODIMENTS OF THE INVENTION

[0031] As described above, the present invention provides demand respirating oxygen supply methods and apparatus for use in sub-acute care which maintain healthy blood oxygen saturation in patients by controlled dosing of oxygen with a measured response to the patient's actual blood oxygen content. The dosing can be provided by simple on/off control over the delivery of oxygen or the amount of oxygen delivered to the patient with each inhalation can be varied in response to the patient's need as determined by a more sophisticated control scheme, such as a proportional-integral-derivative (PID) loop control algorithm, that utilizes the difference between the patient's measured blood oxygen content level and a desired or target blood oxygen content level.

[0032] The systems and methods of the present invention are particularly directed at patients receiving supplemental oxygen in a sub-acute care environment, more preferably in a residential setting. The needs and considerations of patients receiving supplemental oxygen in sub-acute care differ from those present when providing oxygen to patients in critical care environments, in which the amounts of oxygen delivered to patients are carefully controlled in connection with masks or other enclosures that do not typically allow the patents to inspire room air in uncontrolled manners. In those situations, the fractional amount of inspired oxygen (FIO_2) is typically controlled by mixing oxygen and air in a blender or other device before delivering the gas to the patient.

[0033] Among the advantages of the present invention are the significant conservation of oxygen provided by delivering only the amount of oxygen needed to maintain a healthy blood oxygen content and the ability to address therapeutic problems associated with demand delivery systems by providing the correct amount of oxygen to the patient to reduce uncontrolled hypoxic events.

[0034] The amounts of oxygen that can be conserved by implementing the methods according to the present invention can be significant, even compared to known demand delivery systems that conserve oxygen by simply turning the supply on or off during a patient's respiration. Studies have reported oxygen savings ratios of from 3:1 to 7:1 for known simple demand delivery systems. In other words, a fixed amount of oxygen can last three to seven times as long as the same amount of oxygen would last in a supplemental oxygen delivery system that does not include a simple demand delivery system. Implementation of the methods according to the present invention by using a demand delivery approach with a feedback control mechanism that responds to a continuous blood oxygenation measurement could provide an oxygen savings ratio of greater than 13:1 while maintaining the patient's SaO_2 at the 90% level.

[0035] Other advantages of the methods and apparatus according to the present invention are the ability to integrate the invention with any sub-acute care supplemental oxygen supply system, including both ambulatory and stationary sources. For unlimited volume sources, such as oxygen concentrators and membrane separators, the invention will reduce their size and energy consumption for a given level of therapy. For fixed volume gas sources, such as liquid and high pressure gas, the invention will extend the lifetime of the oxygen supply, thereby significantly decreasing the cost of providing that treatment.

[0036] If the system is ambulatory, the present invention can allow for reductions in the size and weight of the oxygen source, thereby increasing the patient's mobility. An added benefit of reducing the size and/or weight of the ambulatory systems is the potential for a better therapeutic outcome. If patients find the smaller, lighter weight systems less cosmetically unattractive they will be more likely to carry and use the systems during ambulatory activities as opposed to not using the systems. Studies have shown that the benefit of supplemental oxygen systems is significantly reduced if the systems are not used on a regular basis.

[0037] Another advantage of the invention, method and apparatus, is a reduction in the risk of hypercapnia (carbon dioxide retention) by only providing enough oxygen to reach a predetermined blood oxygen saturation, typically about 90% as measured by a conventional two-color pulse oximeter.

[0038] One embodiment of an automated respiratory oxygen supply system is depicted in **FIG. 1** and includes a controller **10**, a demand delivery module **12**, and a blood oxygen content sensor **14** connected to the patient **16**. Oxygen is supplied from an oxygen source **20** to the patient **16** by the demand delivery module **12** through, in the preferred embodiments, a supplemental oxygen delivery device **18**. The preferred system may also include a user interface **32** and an alarm **38**.

[0039] The supplemental oxygen delivery device **18** is preferably a nasal cannula as depicted in **FIG. 1**, although it will be understood that the supplemental oxygen delivery device can take the form of any device designed to provide supplemental respiratory oxygen to a patient while not preventing the patient from also inspiring room or ambient air in addition to the supplemental respiratory oxygen from an oxygen source. Examples of other supplemental oxygen delivery devices include, but are not limited to: tracheal catheters, nasal masks designed for use with Continuous Positive Airway Pressure (CPAP) systems, vented masks that cover both the nose and the mouth but that allow inspiration of room air in uncontrolled amounts in addition to the supplemental oxygen delivered to the mask, etc.

[0040] Oxygen source **20** could be an oxygen concentrator, membrane separator, high pressure cylinder or liquid oxygen dewar. This could also include any portable versions of oxygen sources **20**. Other potential sources of oxygen gas suitable for providing supplemental oxygen in sub-acute care in a residential setting and/ambulatory situations may be created in the future and should be considered as being functional with the described invention. As used below, "line" will refer to any connection made between the oxygen source, the described invention and the patient.

[0041] If the oxygen source **20** is an oxygen concentrator, typically a continuous low-flow device, usually delivering at most 6 liters/min of 96% oxygen, the system may also include an oxygen storage device to accommodate the periodic higher flows that are necessary to practice the methods described below. If high flow concentrators become available, such a storage device would not be needed.

[0042] One controller **10** is an electronic circuit including a software programmable microcontroller as its main component. Depending on the allocation of tasks within the device a number of microcontrollers could be used as a controller **10**. In one embodiment, the controller **10** includes a serial data input port, A/D converter, LED driver capabilities and digital I/O pins. One example of a suitable controller is the PIC 16C74A microcontroller from Microchip Technology Inc. of Chandler, Ariz.

[0043] Those skilled in the art will realize that a great deal of optimization may be done relative to the choice of a microcontroller(s). Specifications, such as power consumption, cost, memory size, clock speed and part availability may alter the choice for a preferred microcontroller. Furthermore, many of the functions described for the microcontroller in the preferred embodiment could be accomplished by using discrete circuits of many types. Additionally, the microcontroller and its peripheral circuitry may be replaced entirely by discrete circuitry, such as programmable logic arrays, A/D converter chips, analog comparators, etc.

[0044] The system also includes an oxygen content sensor **14** for monitoring the blood oxygen content of the patient **16**. One suitable sensor **14** includes a sensor control module **14***a* and a sensor **14***b* typically mounted or attached to the patient **16** by some suitable technique. The information from the oxygen content sensor **14** is fed back to the controller **10** for use in executing the methods according to the present invention. It is preferred, but not required, that the oxygen sensor **14** provide a signal to the system controller **10** in the form of a blood oxygen saturation in percent. The sensor **14** preferably, but not necessarily, processes all of its data internally and the controller **10** preferably processes only error flags and numerical information as described shortly.

[0045] One preferred oxygen sensor **14** is a non-invasive sensor such as a two-color pulse oximeter. As used herein, the terms "pulse oximeter" or "oxygen sensor" will include both the optical sensor and the circuitry used to determine blood oxygen saturation levels using the optical sensor. One

example of a suitable pulse oximeter is a conventional two-color, OEM-II oximeter module, from Nonin Medical Inc. of Plymouth, Minn., that can measure the percentage of oxygen-saturated hemoglobin, SpO_2, in the blood stream of an in vivo respiratory system. The preferred embodiment of the pulse oximeter **14** uses a transmitting sensor that attaches to the user's finger. Alternative embodiments may employ sensors that attach elsewhere on the body.

[0046] While the pulse oximeter is one preferred non-invasive oxygen sensor, it should be understood that any blood oxygen sensor, invasive or non-invasive, useful for determining blood oxygen content levels (preferably continuously) could be used in connection with the present invention. It should also be apparent to those skilled in the art that technologies on the horizon, such as an implantable, microelectromechanical (MEMS) blood gas analyzer, may provide the blood oxygen content information needed by the system controller **10**. Furthermore, there may be improvements in pulse oximetry technology, such as the ability to determine the level of carboxyhemoglobin in the blood, that may be useful for the described invention. Use of these new blood oxygen content technologies in oxygen conservers for long-term oxygen therapy should be considered to lie within the scope of the systems and methods of the present invention provided they have the ability to provide suitable blood oxygen content measurements.

[0047] In one embodiment, the pulse oximeter **14** deconvolves the optical information into a blood oxygen saturation value, SpO_2, in percent. The oximeter **14** outputs a serial data stream with this information to the controller **10** for evaluation. Other important information may also be included in the oximeter data stream, such as the user's pulse rate and error flags that detail the reliability of the SpO_2 and pulse rate values.

[0048] It will be recognized by those skilled in the art that an alternative embodiment may be provided in which the system controller **10** functions as the sensor control module **14***a*. As a result, data evaluation and error handling would be accomplished within the system controller **10** with an appropriate oxygen sensor **14***b* being attached to the patient **16**.

[0049] Blood oxygen content measuring in connection with the present invention is described as "continuous" although it will be understood that the measurements made using, e.g., pulse oximeters and other devices, may actually be taken at discrete intervals. As discussed above, "continuous" as used in connection with the measuring of blood oxygen content in the present invention includes measurement of the blood oxygen content levels of the patient at intervals (fixed or variable) that are sufficiently small to provide the advantages of the invention. Preferably the sampling intervals will be less than about five minutes, more preferably less than about one minute, and even more preferably less than about one respiration interval (i.e., the time between the onset of two inhalations by the patient).

[0050] The information relating to blood oxygen content provided by the oxygen sensor **16** is then used by the system controller **10** in combination with the demand delivery module **12** to provide control over the oxygen supplied to the patient **16** from the oxygen source **20** as described in connection with the methods according to the present invention below.

[0051] A block diagram illustrating the components of one embodiment of a demand delivery module **12** according to the present invention is depicted in **FIG. 2**. One component in the demand delivery module **12** is an inhalation or respiration sensor **40** that monitors the respiratory activity of the patient **16** to determine variations in respiration of the patient. It is preferred that the variations in respiration allow the determination of when the patient is inhaling, although other portions of the respiratory cycle may actually be sensed. In other words, inhalation is preferably sensed, but in some cases it may be desirable to determine when inhalation is occurring based on the sensing of some other condition, activity, etc. such as chest movement, exhalation, etc.

[0052] In one embodiment, the respiration sensor **40** provides a signal to a respiration sensor/valve controller **42** that, in turn, controls the valve **26** based on additional input from system controller **10** (as will be described in more detail below).

[0053] The respiration sensor **40** can take a variety of forms that will be known to those skilled in the art. One type of suitable respiration sensor **40** monitors flow in the line used to supply oxygen to the supplemental oxygen delivery device **18**. The sensor **40** in **FIG. 2** monitors flow through the valve **26** interposed in the line between the supplemental oxygen delivery device **18** and the oxygen source **20**. One suitable flow sensor is a Honeywell AWM2150 Microbridge Mass Airflow Sensor (available from Honeywell Corp., Minneapolis, Minn.).

[0054] Another feature of the preferred respiration sensor **40** is the ability to sense bidirectional flow, i.e., flow in each direction through the sensor **40**. It is preferred that the flow generated by inhaling causes a voltage output of one polarity from the sensor **40**, while flow generated by exhaling causes an output voltage of the opposite polarity. In any event, it is preferred that the sensor **40** be capable of detecting both inspiration and expiration.

[0055] In addition to the preferred flow sensor, it should be understood that other types of sensors may be utilized to detect variations in respiration, preferably inhalation and exhalation. Those skilled in the art will recognize that pressure transducers, thermistors or infrared detectors may all be used to sense inhalation. In one example, a pressure transducer with the appropriate sensitivity, such as a solid-state piezoresistive, capacitive or electromechanical device, could be used to generate an electrical signal in response to the breathing cycle. In another example, thermistors could be used to detect changes in airflow due to respiration. If the thermistor was sufficiently sensitive, one may be able to ascertain the onset of inhalation by monitoring the temperature of a thermistor (or thermocouple) placed near the nostril. A flow measurement may also be possible with the use of two thermistors in an anemometer configuration. Infrared detectors, such as single element bolometers, could be used as well if they possess the speed and accuracy to distinguish variations in respiration.

[0056] The respiration sensor **40** provides a signal to the respiration sensor/valve controller **42** which compares the signal to a predetermined reference level. The respiration sensor/valve controller **42** identifies the onset of inhalation by triggering when the sensor signal reaches the predetermined reference level. The respiration sensor/valve controller **42** then provides a signal to position the spool of valve **26** so oxygen flows from supply **20** to patient **16** via

supplemental oxygen delivery device **18**. The spool of the valve **26** remains in this position for a period of time, the "dose time" (D), as specified by the system controller **10**. In this manner, a dose of oxygen of duration D can be provided when the patient is inhaling.

[**0057**] One preferred valve **26** of the embodiment of **FIG. 2** is a three-way, two-position, solenoid-actuated spool valve having three ports **26***a*, **26***b*, **26***c*. Common port **26***a* is connected to the in vivo respiratory system of the patient **16** by the supplemental oxygen delivery device **18**. Normally closed port **26***b* is connected to the oxygen source **20** and normally open port **26***c* is connected to respiration sensor **40** (with the other end of the preferred respiration sensor left open to atmosphere). One preferred valve **26** is manufactured by The Lee Company, of Westbrook, Conn., Model HDI LHDA0523111H.

[**0058**] When oxygen is not being supplied to the patient **16**, the spool of the valve **26** is positioned such that common port **26***a* and normally open port **26***c* are connected so that the respiration sensor **40**, supplemental oxygen delivery device **18**, and patient **16** are in fluid communication, corresponding to the OFF position of the valve **26**. This allows the respiratory effort of the patient **16** to be detected by the respiration sensor **40**, through the monitoring of the flow generated in the supplemental oxygen delivery device **18** by inspiratory and expiratory efforts.

[**0059**] To supply oxygen to the patient **16**, the spool of the valve **26** is moved so as to connect common port **26***a* and normally closed port **26***b*, corresponding to the ON position of the valve **26**. This, in turn, allows for flow of respiratory oxygen to the patient **16** from supply **20** through the valve **26** and the supplemental oxygen delivery device **18**.

[**0060**] The ON period for the valve **26**, corresponding to the dosage period as discussed below, is preferably shorter than the inhalation period for the patient. As a result, the patient may often be inhaling after the valve **26** is OFF (i.e., closed). To reduce or prevent multiple openings of the valve **26** during a single inhalation, it is preferred that the valve **26** remain closed until the sensor **40** detects the onset of exhalation. Once exhalation is detected based on the sensor **40**, the system can then resume monitoring for the onset of inhalation, whereupon the cycle is repeated.

[**0061**] Because the preferred valve **26** is a 3-port valve, there is a short period after opening or closing the valve **26**, (the "bounce period") where the sensor output voltage spikes or bounces due to oxygen leaking from the normally closed port **26***b* to the normally open port **26***c* while the valve spool is still moving. Once the valve **26** is fully ON or OFF and the valve spool has stopped moving, the bounce signal disappears. It is preferred that monitoring of the respiration sensor **40** be adjusted to avoid false readings due to the bounce signal after turning the valve **260**N or OFF. This adjustment can take the form of a delay in monitoring the signal provided by the sensor **40** after moving the valve **26** between the ON and OFF positions until the bounce signal has passed.

[**0062**] In some systems, the bounce signal may be monitored and used advantageously. The bounce signal (whether generated during ON or OFF movement of the valve spool) may be used to detect the presence of oxygen at the supply **20**. No bounce signal may indicate that no oxygen is present because of the lack of pressurized oxygen at normally closed port **26***b*. In the preferred embodiment, the bounce signal generated by turning the valve **26** to the OFF position (i.e., closing port **26***b*) is used for this check because that bounce signal is typically larger and longer in duration than the bounce signal generated by turning the valve **26** to the ON position (i.e., opening port **26***b*).

[**0063**] Another advantage of the 3-port valve **26** is that sensor's zero-flow offset voltage can be checked while the valve **26** is in the ON position. The measured sensor offset voltage signal (Vo) can be used to generate a correction for drift in the sensor offset voltage. After the valve **26** has been ON longer than the valve-ON bounce period, the signal from the respiration sensor **40** can be read and recorded for use in, e.g., a software-generated correction for zero-flow sensor offset voltage. This sensor offset voltage signal is obtained from the respiration sensor **40** when the valve **26** is ON because no flow is to be expected through the respiration sensor **40** under those conditions (port **26***c* is closed). In addition, if this offset reading is greater (in absolute value) than a predefined upper limit (VoMAX), this can be used to indicate either sensor **40** or valve **26** failure; e.g., the sensor **40** has drifted too far out of specification, the valve **26** is leaking, the valve **26** is stuck in the OFF position, etc.

[**0064**] The demand delivery module **12** described above is a subsystem that communicates to and receives communication from system controller **10**. In the described methods, it receives continually updated values of the dose time D. It will be understood, however, that those skilled in the art could design a demand delivery module **12** which is more or less dependent on the system controller **10** than is described in this embodiment. For example, it may be desirable to construct a system where respiration sensor **40** provides a signal directly to the system controller **10** with no separate respiration sensor/valve controller **42** being provided. The controller **10** would then provide a control signal to valve **26** directly as well as perform the other operations that are described as being performed by the respiration sensor/valve controller **42**.

[**0065**] Moreover, it should be understood that alternative designs for the connections of the valve **26**, respiration sensor **40**, oxygen source **20**, and patient **16** may be envisioned by the those skilled in the art. It would be possible to design a system in which an in-line flow sensor and/or three-port, two-way valve are not required. For example, the designs may involve a plurality of valves and sensors. It should be understood that the methods and systems of the described device operate independently from the specific configuration of hardware used for sensing variations in respiration and the specific valve configuration used to control the flow of oxygen.

[**0066**] Although the demand delivery module **12** described above is used to control delivery of supplemental oxygen to a patient from the source **20**, the demand delivery module **12** and the methods of operating it as described above could find wider application. For example, they could be used in connection with critical care systems in which FiO_2 is to be controlled via the use of masks or other delivery devices used in connection with, e.g., respirators, ventilators, BIPAP (Bilevel Positive Airway Pressure) systems, etc. As a result, the demand delivery module and methods of operating it are not to be limited to use in connection with

systems and methods of delivering supplemental oxygen as part of a sub-acute care regime.

[0067] As long as the data stream from the blood oxygen content sensor **14** is valid (as described in detail below), the controller **10** can use the data to control delivery of oxygen to the patient. The feedback control can be implemented as a portion of software code contained in the controller **10**; however, it could alternatively be a hard-wired controller or combination of hardware and software in other embodiments.

[0068] There exist a variety of control methods that are of utility in the present method and invention. The goal of any control method is stable operation of the controlled system about a setpoint or desired value. In the preferred embodiment, the desired value is a blood oxygen saturation (SpO_2) of 90%. One control algorithm, the ON/OFF method, is diagrammed in **FIG. 3***a*. This diagram assumes that the data generated by the blood oxygen content sensor is valid (validity and invalidity of that data is discussed in more detail below).

[0069] The system measures the patient's blood oxygen content level **100**. With that information, a decision **102** is made. When the measured blood oxygen content level is not below the desired value no oxygen is delivered **104**. When the measured blood oxygen content level is below the desired value, oxygen is delivered **106**. For example, when the measured blood oxygen content level is not below the desired value, controller **10** sets a dose time of zero (D=0), thereby preventing the delivery of supplemental oxygen. Alternatively, the system may otherwise restrict the flow of oxygen by, e.g., reducing its flow to a very low value in an attempt to conserve the supplemental oxygen source. The reduction in flow can be accomplished using a variable flow valve or by introducing a flow restrictor into the system between the source **20** and the patient **16**. When the measured blood oxygen content falls below the desired value, controller **10** delivers supplemental oxygen to the patient **16** by, e.g., setting a non-zero value (D>0) for the dose time or otherwise increasing the flow of oxygen to the patient.

[0070] As long as the measured blood oxygen content level remains below the desired value, the system provides oxygen when the patient is inhaling. In one relatively simple implementation, the "ON" dose time D could be very long. Preferably, however, the dose time is equal to or shorter than a typical inhalation period, in which case one or more pulses of duration D of oxygen are delivered during inhalation. This ON/OFF control approach is analogous to the operation of a furnace using a mercury switch thermostat, i.e., oxygen delivery is either ON or OFF.

[0071] The feedback control algorithm may alternatively use a Proportional-Integral-Derivative (PID) loop as illustrated in **FIG. 3***b*. Other embodiments could use algorithms based on fuzzy logic, look-up tables, P or PI loops or increment/decrement methods (oxygen delivery that increases or decreases in a preprogrammed fashion relative to setpoint and/or trend). The PID algorithm is fundamentally different from the simple ON/OFF control algorithm in that it uses both the current value of the blood oxygen content and also trend information to determine whether the patient needs supplemental oxygen and, if so, how much oxygen should be delivered when the patient is inhaling. Because of the use of trend information, a system controlled with a PID loop will, at times, deliver oxygen to the patient even if their blood oxygen content is above the desired value; or, at other times, it may not deliver oxygen even if they are below the desired value. An example of when this might occur is when the patient's blood oxygen content was above the desired value, but was also dropping very quickly. In this case, the PID loop would start oxygen delivery before the blood oxygen content actually fell below the desired value. (The ON/OFF method would not start oxygen delivery until after the blood oxygen content was below the desired value). This may allow a PID control method to more effectively reduce the fluctuations of the blood oxygen content about the desired value.

[0072] A simplified flow diagram of one such PID control system is illustrated in **FIG. 3***b* where the data stream of the measured blood oxygen content level sensor is assumed to be valid (validity/invalidity of that data is discussed in more detail below). The system measures the patient's blood oxygen content level **110**. The current information is compared with earlier data **112** to determine how much oxygen (i.e., a variable dose), based on the parameters of the PID loop **114**, should be delivered to the patient **1116**. In some instances, the parameters of the PID loop indicate that no oxygen is to be delivered **118**, and in other instances some variable dose of oxygen will be delivered based on the parameters of the PID loop.

[0073] The preferred systems for implementing the methods of the present invention use a digital controller. As a result, discretization of the following continuous-time PID control equation must be performed:

$$D(t)=K_p*[e(t)+(1/T_i)*\int e(t')dt'+(T_d)*de/dt] \quad (1)$$

where D(t) is the oxygen dose time at time t, K_p is the loop proportional gain, T_i is the integral time, T_d is the derivative time, and where the integral is integrated over the range of from zero to t. The preferred embodiment utilizes a first order discretization of the continuous time PID equation. This can be seen in Equation 2,

$$D(t_n)=D(t_{n-1})+A_0e(t_n)+A_1e(t_{n-1})+A_2e(t_{n-2}) \quad (2)$$

where $D(t_n)$ is the control signal (oxygen dose time) generated for time period t_n, $e(t_n)$ is the difference between the desired level of blood oxygen saturation (the setpoint) and the measured level at time t_n. The coefficients, A_0, A_1, and A_2 are given by Equations 3-5 below:

$$A_0=K_p*(1+t_n/t_i+t_d/t_n) \quad (3)$$

$$A_1=-K_p*(1+2*t_d/t_n) \quad (4)$$

$$A_2=K_p*(t_d/t_n) \quad (5)$$

where K_p is the loop proportional gain, t_i is the integral time, t_d is the derivative time and t_n is the period of the measurement (one second if using the preferred oximeter).

[0074] As mentioned, the quantity $e(t_n)$ is the difference between the SpO_2 value at time t_n and the desired value. In one embodiment, a fixed setpoint of SpO_2=90% is used for the desired value. The control algorithm will specify doses of oxygen in order to maintain the blood oxygen saturation at this level. It is thought that this saturation level may provide the necessary correction to the patient's hypoxemia, while at the same time conserving the greatest amount of oxygen. It should be apparent to those skilled in the art that the desired value (setpoint) can be changed to achieve different therapeutic and economic goals.

[0075] Moreover, a system that uses additional physiological parameters, such as pulse rate or respiratory rate, in addition to blood oxygen content as determined by the oxygen sensor to determine a target blood oxygen level (setpoint) that changes on a rolling basis could also be implemented. For example, one may use the heart rate to monitor the patient's activity level and therefore anticipate increased or decreased need of oxygen and adjust the setpoint accordingly. Such schemes would be seeking to ameliorate the possible increased/decreased hypoxemia caused by a change in physical activity level. Such changes to the setpoint should be considered to be within the spirit and scope of the present invention.

[0076] Referring now to Equations 3-5 above, the transfer function coefficients A_0, A_1 and A_2 are determined by the settings of loop proportional gain K_p, the integral time t_i, the derivative time t_d and the time between data points t_n. The determination of these values will typically be accomplished through clinical monitoring of COPD patients while the system is in use. The specific values of these loop parameters will depend on design goals such as loop stability, overshoot, time-to-achieve-control, and accuracy. Methods for obtaining values which provide for effective operation of the control loop will be known to those skilled in the art.

[0077] In one method, the control signal $D(t_n)$ is the dose time needed to maintain the blood oxygen level at the desired value. The dose time signal is provided by controller **10** to respiration sensor/valve controller **42**. It is the duration of time that valve **26** will be held in the ON or open position which permits oxygen to pass from supply **20** to patient **16** (via the supplemental oxygen delivery device **18** illustrated in **FIGS. 1 and 2**). A dose of oxygen of duration $D(t_n)$ is provided during inhalation (as indicated by respiration sensor **40** and sensor and valve controller **42**, described previously).

[0078] It should be understood that other methods besides varying the dose time could also be employed to control the patient's blood oxygen content. For example, a system which includes a variable-flow valve (as opposed to the preferred open/closed valve) could be constructed. In such a system, the controller **10** could specify the oxygen flow level. The specified flow could, in turn, be provided for a fixed period of time at the onset of each breath, or continuously. During those times in which the patient does not require supplemental oxygen and/or is not inhaling, the flow could be restricted to a low level or to zero followed by periods in which the flow is higher (when the patient is in need of supplement oxygen and is inhaling).

[0079] Alternately, the blood oxygen content could be controlled by providing a dose of oxygen on one or more sequential breaths and then delivering no oxygen on one or more subsequent breaths. In this method, the control parameter could be described as the number of breaths during which oxygen is or is not delivered. It should be understood that those skilled in the art could construct a control scheme which uses any of these alternate methods or a combination of these methods.

[0080] The controller **10** also may include a minimum limit (Dmin) for the dose time. If the dose time $D(t_n)$, as determined by Equation 2, is less than Dmin, a dose time of Dmin will be used instead. In one embodiment, Dmin will be zero. The dose time $D(t_n)$ determined by Equation 2 will, at times, be negative. This will primarily occur when the patient's blood oxygen content is greater than the desired value. Since a negative dose time is not physically meaningful, the controller will instead substitute a dose time of Dmin. Of course, Dmin could also be greater than zero.

[0081] Similarly, in one embodiment the controller **10** would also have a maximum limit (Dmax). If the dose time $D(t_n)$, as determined by Equation 2, is greater than Dmax, a dose time of Dmax is used instead. In one embodiment, Dmax is equal to twice the default dose (described in detail below). This prevents the application of excessive amounts of oxygen and thus minimizes the patient's risk of hypercapnia (carbon-dioxide retention). Those skilled in the art will appreciate that other values of Dmax could also be used.

[0082] In another embodiment, the controller **10** could include an "anti wind-up" provision. Because the dose time may have minimum and maximum limits (Dmin and Dmax, described above), it may be advantageous to include an anti wind-up provision to prevent the integral portion of the PID-calculated dose time from getting too large or too small. One way this could be implemented is as follows: If the previous PID-calculated dose time $D(t_{n-1})$ (from Equations 2-7) is less than Dmin or greater than Dmax, the integral term from Equation 3 is deleted (i.e., Equation 3 is replaced with Equation 3a, below):

$$A_0 = K_p * (1 + t_d / t_n) \quad (3a)$$

[0083] In systems and methods according to the present invention, the ability to respond to periods of invalid or bad data in the blood oxygen content measurements is preferably provided. In the preferred methods and systems, the delivery of oxygen moves from the closed loop control described herein to open loop control based on the criteria described herein (i.e., default values, interpolated data, etc.) and back to closed loop control when the blood oxygen measurements are again valid. **FIG. 4** illustrates these concepts. As shown, the system obtains a measured blood oxygen content level **120**. A decision is then made as to whether the measured blood oxygen content level data is valid or invalid **122**. The system may determine whether the measured blood oxygen content level data is invalid on a point-by-point basis or it may determine whether the data stream (including a plurality of data points) is invalid as discussed below. Regardless, a decision will be made as to whether the measured blood oxygen content level data is valid. If the measured blood oxygen content level data is invalid, the system will deliver a default amount of oxygen to the patient **124**. If the measured blood oxygen content level data is valid, the system will deliver oxygen to the patient **126** according to the appropriate control algorithm (ON/OFF, PID loop, etc.).

[0084] In other words, the methods/systems according to the present invention will determine when the blood oxygen content data is invalid, deliver a default amount of oxygen during periods of invalid data, and then resume delivery of supplemental oxygen based on blood oxygen content when that data is again valid. The ability of the systems and methods of the present invention to move from closed to open and back to closed loop control provides a robust system that can operate with a minimum of supervision from medical personnel. Those qualities are essential in any system designed for residential or ambulatory use by subacute patients.

[0085] The following description illustrates some preferred methods for accomplishing these features, but it

should be understood that in its essence the present invention provides for that movement from closed loop control to open loop control and back to closed loop control based on the presence of valid or invalid blood oxygen content measurements.

[0086] In one embodiment, before the measured blood oxygen saturation reading ($Sp0_2$) is used for determining the dose time D of oxygen to be delivered to the patient **16** from the oxygen source **20**, various error handling and artifact detection procedures are followed to prevent erroneous over- or under-dosing of oxygen to the patient. In one embodiment of the present invention, the error flags provided by the oxygen sensor **14** in the serial data stream are combined with a numerical analysis of the $Sp0_2$ data to create an artifact detection and handling scheme.

[0087] The serial data stream of the preferred pulse oximeter **14** provides one data point per second. Each data point includes three bytes of information, as follows:

1st byte = Status	Bit 7 = Always set to "1" Bit 6 = Sensor disconnected, set if true Bit 5 = out of track, set if true Bit 4 = low perfusion, set if true Bit 3 = marginal perfusion, set if true Bit 2 = bad pulse, set if true Bit 1 = heart rate bit 8 Bit 0 = heart rate bit 7
2nd byte = Heart Rate	(511 = bad data) Bit "7" is always set to "0" Heart Rate Data = Bits 0–6 Plus bits 0 & 1 of status byte to provide 9 bits of resolution
3rd byte = SpO_2	(127 = bad data)

[0088] The first byte of the data point may include error flags for some problems associated with pulse oximetry. These flags are examined for the occurrence of a disconnected sensor, low or marginal perfusion, out of track oximeter and bad pulse. If any of these flags are set, the accompanying SpO_2 and heart rate data is considered bad. If the data point is determined to be bad, a timer (Timer1) is started by the controller **10** (unless it is already running based on an earlier bad data point) which then waits for the next data point. The function of Timer1 is to track the cumulative time over which consecutive bad data points are being received. Timer1 is stopped and reset to zero each time a valid or good data point is received.

[0089] If, however, none of the flags is set, a second error check may be performed using a statistical analysis of the data. The new data point is compared to a mean value of previous data points which represents the patient's current blood oxygen content. The details of the calculation of this mean value are described below. The current data point is subtracted from the mean value to generate a difference, ΔSpO_2 in %. (For the data-validity analysis below, if ΔSpO_2 is less than zero, its absolute value is used.)

[0090] If the absolute value of ΔSpO_2>4% and Timer1 equals zero (i.e., the last data point was valid), then the current data point is determined to be invalid. Since the time between data points in the serial data stream will be about one second, a change larger than 4 percent in the SpO_2 in such a short time would be physiologically impossible. If the data point is determined to be invalid using this procedure, the data is ignored, Timer1 is started and controller **10** waits for the next data point.

[0091] If, however, the absolute value of ΔSpO_2>4% and Timer1 does not equal zero, then additional evaluation may be performed. The observed rate of oxygen desaturation in humans can approach 20%/minute or about 3% every 10 seconds. If Timer1 is less than 10 seconds and the absolute value of ΔSpO_2>4%, then the data is considered to be invalid. If Timer1 is greater than 10 seconds, but less than 20 seconds then the acceptance criteria is absolute value of ΔSpO_2 less than 8% for the data to be valid. If Timer1 is greater than 20 seconds, but less than 30 seconds then the acceptance criteria is absolute value of ΔSpO_2 less than 12%. If Timer1 is greater than 30 seconds, then oxygen is delivered using the default method which is described in detail below. It should, of course, be understood that, in the above analysis, the specific values of 4%, 8%, and 12%, and the specific times of 10, 20 and 30 seconds could be replaced with different values.

[0092] Some alternate criteria for identifying when individual data points are invalid or bad could include, but are not limited to, identifying an invalid data point when: (a) the SpO_2 value is outside upper and/or lower limits (e.g., a lower limit of about 70% and/or an upper limit of about 98%); or (b) the heart rate is outside upper and/or lower limits (e.g., a lower limit of about 40 beats per minute and/or an upper limit of about 200 beats per minute).

[0093] If the data point passes all the tests, Timer1 is stopped and set to zero (if necessary) and the new mean value of blood oxygen content is calculated with the most recent data point. The new mean value is then compared to the setpoint and a dose time D is calculated as detailed above in Equations 2-5.

[0094] In one embodiment, an exponentially-weighted arithmetic mean of the previous data points is used to represent the current blood oxygen content. The new mean is calculated as follows:

$$\text{new mean}=(\text{current data point})*W1+(\text{previous mean})*W2 \quad (6)$$

where

$$W1=1-\exp(-\Delta t/T)\ \ W2=\exp(-\Delta t/T). \quad (7)$$

Here Δt is the time between data points (one second using the preferred oximeter), and T is a parameter which represents an appropriate time scale for the averaging. If an appropriate value of T is chosen, the exponentially-weighted mean will smooth out normal point-to-point "noise" fluctuations in the pulse oximeter data without masking the real trends related to the patient's blood oxygen content. (A typical value would be T=10 seconds, although other values could be used.)

[0095] Other methods could also be used to determine a mean value that is representative of the patient's current blood oxygen content. For example, a harmonic, or geometric mean might be used. (Descriptions of these types of means can be found in "Standard Mathematical Tables" by CRC Press, 24th edition, pages 470-471.) Alternately, a "running" mean might be used. In this method, the mean of a fixed, predetermined number of the most-recent data points could be used. For example, with the preferred pulse oximeter which delivers one data point per second, one

could average the preceding 10 data points, thus calculating a mean which represents the patient's blood oxygen content for the previous 10 seconds.

[0096] In one embodiment, the dose time D of oxygen that is delivered to the user may depend on the validity of the data stream from the oxygen sensor. If the time over which the consecutive invalid or bad data points are received, as indicated by Timer1, exceeds a predetermined, physiologically-relevant time scale for patient desaturation (referred to as Desattime), alternative, "default" oxygen delivery procedures are employed. In one embodiment Desattime is equal to 30 seconds. The default assumption is that a patient is always in need of oxygen, unless the blood oxygen content sensor positively indicates that they are not.

[0097] If the current oxygen sensor data point is invalid, but Timer1 is less than Desattime, the oxygen dose time D may remain unchanged from its current value. The system will provide a dose of this duration at the onset of inhalation. The process of gathering and evaluating blood oxygen saturation data then continues. Prior to the onset of invalid data, the system was either administering oxygen to correct a deficiency or the patient was in no need of oxygen. Thus, in this embodiment it is assumed that the patient's oxygen needs have not changed during this short time of invalid data and the status quo is maintained. If the patient was receiving no oxygen prior to the invalid data (e.g., dose time D=0), the system will not administer any oxygen. If, however, the patient was receiving oxygen (e.g., D>0), the system will typically continue to administer the same dose by responding to inhalation as described above. This will preferably continue until either a valid data point is received and a reevaluation can be made of the patient's condition or Timer1 exceeds Desattime.

[0098] If the oxygen sensor data points continue to be invalid and Timer1 exceeds Desattime, then the device will default to another oxygen delivery method. In the default method, the controller **10** will default to administering a prescription-equivalent dose of oxygen to the patient **16** from the oxygen source **20** via the demand delivery module **12**. This default dose of oxygen could take many forms: In one embodiment, the default could be a continuous flow of oxygen. To implement this, the system could output a very large dose time to hold valve **26** in the ON position which allows oxygen to flow from source **20** to patient **16**. Alternately, in the preferred embodiment, the default mode would provide a short dose of oxygen (of duration D=Ddefault) at the onset of inhalation for almost every breath. In this preferred embodiment, Ddefault would be shorter than a typical inhalation period, in which case the system would provide pulses of duration Ddefault synchronized with each inhalation (demand mode). This will continue until such time as the blood oxygen content data is valid and closed-loop control over oxygen delivery can start anew.

[0099] It is possible to envision additional alternate methods of default flow. In one such alternate embodiment, the valve does not necessarily open with each and every breath. It should be understood that these alternate methods of implementing a default flow still fall within the scope of the present invention. The object of the default method is to provide a total flow of oxygen during this period of default operation that is no less than the physiological equivalent amount that is prescribed to the patient by the physician. (Physiological equivalence meaning the amount dispensed by other demand delivery devices to provide adequate oxygen therapy.) It should be understood that the notion of physiological equivalence as regards demand delivery devices will change over time as their effects on the physiology of COPD patients is better understood by the medical community. Current practice indicates that 35 ml delivered every other breath at the beginning of inhalation is equivalent to a continuous flow of 2 liters/minute of pure oxygen.

[0100] In one embodiment of the invention, the duration of the default dose (Ddefault) may be set by the patient's respiratory therapist using a hardware switch on the user interface **32** that is not accessible to the patient. Other techniques of setting the pulse width may be possible, such as a remote controllers, push buttons, etc.

[0101] Also, in one embodiment, if Timer1 exceeds Desattime, then the previous mean value of the blood oxygen saturation is reset and data acquisition starts anew. In this way, it is assumed that the old SpO_2 information is no longer valid for the patient's current physical state and that to properly administer oxygen a more current measure of the blood oxygen level is needed. Thus, by using Timer1, a period of invalid data that exceeds Desattime will always lead to the administration of oxygen to the patient. This will correct any undetected desaturation events. Moreover, the controller **10** will always use the most current, valid information regarding the patient's blood oxygen level.

[0102] It should also be understood that other methods for recognizing and handling erroneous data points from the oxygen sensor could be devised. Those skilled in the art could create different algorithms for handling invalid data points, such as replacement of invalid data points with interpolated values based on the recent trend in the blood oxygen saturation. Alternative methods of identifying and rejecting invalid data points should be considered to be within the scope of the present method and system.

[0103] Another method for determining whether the oxygen sensor data is valid or invalid can be based on the data stream (a plurality of data points) rather than the individual data points. For example, instead of tracking the time since the most recent valid data point or points, the system could instead determine if the data stream is valid or invalid by comparing the number of valid data points in a "look-back" window (for example, the 60 to 100 most recent data points) to a preset minimum threshold. If the number of valid data points in the look-back period is greater than or equal to the specified minimum, the data stream is considered to be valid and the calculated dose is delivered; if the number of valid data points is less than the minimum, the default dose is delivered.

[0104] Those skilled in the art will understand that a wide range of possibilities for oxygen delivery in default mode beyond those that have been described here could be used. Although they are not described in detail herein, they should be considered as falling within the scope of the methods according to the present invention.

[0105] If invalid data is a problem, the controller **10** may be used to notify the patient of a problem with the pulse oximetry via the user interface **32** and/or alarm **38**. This notification may take the form of a warning light, readout, buzzer or some combination of these. Those skilled in the art

may also conceive of other methods of warning the user that are not detailed herein. After the warnings have been issued and default demand flow mode entered, the controller **10** resumes monitoring the output of the oxygen sensor for valid data.

[**0106**] Along with monitoring the breathing cycle for oxygen delivery, the invention makes provision for the detection of apnea, the cessation of breathing for a prolonged period of time. Timer2 starts each time an inhalation is detected. If the elapsed time between breaths is greater than a predetermined time, e.g., 15 seconds, as determined by Timer2, then the alarm circuit **38** is activated by the controller **10** to signal the patient of a possible apneic event. These alarms preferably stop sounding upon detection of the next inhalation.

[**0107**] Other alarms and indicators that can be included in the systems and methods of the present invention include hypoxia alarms, high respiration rate alarms, high/low pulse rate alarms, and patient monitoring indicators. These alarms and/or indicators can be used to warn the patient that their supplemental oxygen equipment is not operating properly, they are not using it properly, or they are having other problems and need to seek medical treatment.

[**0108**] In the case of an hypoxia alarm, the patient could be provided with a visible and/or audible alert when their blood oxygen saturation level has been below a healthy level for a period of time—even though they have been using the above-described device. This condition could be caused, e.g., by a malfunctioning of the supplemental oxygen equipment or a worsening of the patient's respiratory condition. In normal operation of the preferred embodiment as described above, the device would increase the dose time D(t) in response to the patient's hypoxia, up to a preset upper-limit dose time Dmax. It is possible that the patient's condition could have worsened so much so that even this maximum dose is not sufficient to keep their blood oxygen saturation at a healthy level. It would be advantageous to alert the patient to this condition so they may seek appropriate medical attention. This could enable earlier detection and treatment of potentially dangerous and costly health conditions.

[**0109**] The hypoxia alarm could be implemented in software, hardware, or in a combination of software and hardware. In the methods described above, the controller **10** may already calculate a mean value of blood oxygen content from the valid blood oxygen saturation data points. In the preferred embodiment, the mean value that is already calculated is an exponentially-weighted arithmetic mean with a typical time constant T=10 seconds. This mean represents the average blood oxygen saturation for the previous 10 seconds. For the hypoxia alarm, a second mean value of blood oxygen saturation, for a longer period (e.g. T=1 hour) could be calculated in an analogous manner. In the preferred embodiment, this hypoxia alarm mean would also be an exponentially-weighted mean because it eliminates the need to store each of the many data points that would be collected over the longer period, thereby decreasing the memory requirements.

[**0110**] It should be understood, however, that other methods of calculating a mean as discussed above could also be used. When the second mean falls below a preset limit representing the lower limit for healthy blood oxygen levels (e.g., 88%), controller **10** could alert the patient via alarm circuit **38**. In the preferred embodiment, the time period for the second mean is 1 hour, and the lower limit for blood oxygen saturation is 88%; however, it should be clear that other values could be used for these parameters.

[**0111**] In the case of a high respiration rate alarm, the patient could be provided with a visible and/or audible alert when their respiration rate has been above a healthy level for a period of time. Some patients with respiratory diseases will compensate for an impaired respiratory system by maintaining a higher than normal breathing rate. These patients can sometimes maintain a healthy blood oxygen saturation, but over the long term, the increased respiration rate is also detrimental to their health. The onset of a period of increased respiration rate could be caused by a malfunctioning of the supplemental oxygen equipment or a worsening of the patient's respiratory condition.

[**0112**] In normal operation of the preferred embodiment as described above, the device increases the dose time D(t) in response to the patient's hypoxia. It is possible that the patient's condition could have worsened, but the patient is compensating by breathing at a higher rate. As with hypoxia, it would be advantageous to alert the patient to this condition so they may seek appropriate medical attention.

[**0113**] This alarm could be implemented in software, hardware, or in a combination of software and hardware. The system described above already measures the elapsed time between each breath via Timer2. For the high-respiration rate alarm, a mean value of the elapsed time between each breath could be calculated in a manner analogous to the mean blood oxygen levels. In the preferred embodiment, this mean would also be an exponentially-weighted mean. It should be understood, however, that other methods of calculating a mean as described above could also be used. When the mean elapsed time between breaths falls below a preset limit corresponding to the upper limit for healthy respiration rates (e.g., minimum elapsed time of two seconds, corresponding to a breathing rate of 30 breaths per minute), the system could alert the patient via controller **10** and alarm circuit **38**. In the preferred embodiment, the time period for calculating the mean is 1 hour, and the lower limit for elapsed time between breaths is 2 seconds (30 breaths per minute); however, it should be clear that other values could be used for these parameters.

[**0114**] In the case of a high/low pulse rate alarm, a visible and/or audible alert could be provided to the patient when their pulse rate has been above or below healthy levels for a period of time. Excessively high or low pulse rates could be an important indication that the patient needs medical treatment. It would be advantageous to alert the patient to these conditions so they may seek appropriate medical attention.

[**0115**] In the preferred embodiment, these alarms would be implemented in software, hardware, or in a combination of software and hardware. The preferred oxygen sensor typically provides pulse rate data (in addition to blood oxygen data). A mean pulse rate could be calculated in a manner analogous to the calculation of other means, described above. As with the other alarms, in the preferred embodiment, this mean would also be an exponentially-weighted mean or, alternatively, other means or averages could be used.

[0116] When the mean pulse rate falls above or below preset limits (e.g., less than 40 or above 180 beats per minute), the system could alert the patient via alarm circuit **38**. In the preferred embodiment, the time period for the mean is 20 minutes, the lower limit for pulse rate is 40 beats per minute, and the upper limit for pulse rate is 180 beats per minute; however, it should be clear that other values could be used for these parameters.

[0117] Among the indicators that could be provided include various patient and equipment monitoring functions. In the preferred embodiment, these indicators could be implemented in software, hardware, or in a combination of software and hardware. The information provided by these indicators could be useful to the patients, respiratory therapists, physicians, etc. Some examples of indicators are described below.

[0118] One indicator that could be useful is an "ON-time" indicator. An important factor in treating patients that require supplemental oxygen is monitoring their compliance with their oxygen prescription. Some patients will not use their oxygen equipment as much as they should. Medical studies have shown that most patients must use their supplemental oxygen equipment at least 18 hours per day in order to receive significant benefits from it. The ON-time parameter would indicate the total amount of time that the device has been powered ON (analogous to the "hour meter" found on most oxygen concentrators), thus giving an indication of the total time the equipment was used since the ON-time parameter was last reset to zero. In the preferred embodiment, a timer would be started by controller **10** each time the unit was turned ON. When timer reached a value of, e.g., one minute, controller **10** would increment a non-volatile memory location and reset and restart the timer. In this manner, a memory location associated with the ON-time timer would count the number of minutes the apparatus had been powered ON. The memory location associated with the ON-time timer would preferably be non-volatile and, as a result, the total minute count would be retained while the unit was powered OFF. When powered ON again, counting would resume from the previously accumulated value. In the preferred embodiment, the ON-time timer could be accessed and reset via the user interface **32**.

[0119] It may also be useful to track the total number of times each alarm condition has occurred. In the preferred embodiment, a separate non-volatile memory location would be used to count the number of times each alarm condition had occurred. Each time an alarm condition occurred, the associated memory location would be incremented. In addition to the three alarms described above, the preferred embodiment could also count the number of apnea alarms. The various alarm-count parameters could be accessed and reset, e.g., via the user interface **32**.

[0120] It may also be useful to keep track of the total amount of time the unit was in "default" mode as described above. In a manner similar to tracking ON-time, the default time monitor would preferably consist of a non-volatile memory location that would be incremented each time the timer reached one minute and the unit was in the default mode. In a similar manner, a feedback-control-time parameter could be calculated (although this parameter may be more easily obtained by subtracting the default time from the ON-time). As with the other monitored parameters, default time would preferably be accessed and reset via the user interface **32**.

[0121] It may also be useful to keep track of the total number of times the apparatus entered the "default" mode. In the preferred embodiment, a separate non-volatile memory location would be used to count the number of times the default delivery condition had occurred. Each time the apparatus entered the default delivery mode, the associated memory location would be incremented. The default count parameter would preferably be accessed and reset via the user interface **32**.

[0122] It may also be useful to keep track of the total amount of time the patient was hypoxic (e.g., SpO_2<88%). In a manner similar to tracking the ON-time, the hypoxic-time monitor would consist of a non-volatile memory location that would be incremented each time the timer reached one minute and the patient was hypoxic (and the SpO_2 data was deemed valid). As with the other monitored parameters, hypoxic-time could be accessed and reset via the user interface **32**.

[0123] It may also be useful to keep track of the average duration of the pulses of oxygen that are provided at each inhalation (i.e., the average dose time). The average-dose-time parameter could provide a useful indication of the amount of supplemental oxygen that was required to keep the patient's blood properly oxygenated. Trends in this parameter could be useful for tracking the overall efficiency of the patient's respiratory condition. For example, a measurable increase in the average-dose-time (i.e., an increase in the amount of supplemental oxygen needed) could indicated a worsening of the patient's condition, and thus provide an early warning allowing the patient to seek medical attention before their condition required a costly hospitalization.

[0124] In the preferred embodiment, two nonvolatile memory locations would be used to calculate average-dose-time: a counter and an accumulator. Each time, e.g., an inhalation was sensed, the current dose time (as indicated by controller **10**) would be added to accumulator and the counter would be incremented. The average-dose-time could then be calculated by dividing the accumulator value by the counter value. As with the other monitored parameters, average-dose-time could be accessed and reset via the user interface **32**.

[0125] In addition to those parameters specifically recited herein, other useful parameters may also be generated. For example, average SpO_2 (the patient's average blood oxygen saturation); average respiration rate; average heart rate; etc. Monitoring of these parameters could also be implemented in software, hardware, or in a combination of software and hardware.

[0126] Various methods and systems for conserving supplemental oxygen delivery to a sub-acute patient based on continuous blood oxygen content measurements and inhalation have been described above. Many changes, alterations and variations of the subject invention will become apparent to those skilled in the art after consideration of this specification and the accompanying figures and diagrams of the preferred embodiments. For example, the values chosen for, e.g., ΔSpO_2, Timer1, Timer2, etc., are intended to be exemplary of some preferred values and should not limit the

scope of the invention unless the values are explicitly recited in the claims. All such changes, modifications, variations, etc. are deemed to be covered by the claims which follow.

1. A method of controlling oxygen delivery comprising:

continuously measuring blood oxygen content of a patient to obtain a measured blood oxygen content level;

delivering oxygen from an oxygen source to the patient if the measured blood oxygen content level is below a desired value;

restricting the delivery of oxygen to the patient if the measured blood oxygen content level of the patient is above the desired value;

determining if the measured blood oxygen content level is invalid; and

delivering a default amount of oxygen to the patient if the measured blood oxygen content level is invalid.

2. A method according to claim 1, wherein the oxygen is delivered through a nasal cannula.

3. A method according to claim 1, further comprising determining when the patient is inhaling.

4. A method according to claim 1, further comprising providing an alarm if the measured blood oxygen content level is invalid.

5. A method according to claim 1, further comprising providing an alarm if the patient experiences hypoxemia.

6. A method of controlling oxygen delivery comprising:

continuously measuring blood oxygen content of a patient to obtain a measured blood oxygen content level;

delivering a variable dose of oxygen from an oxygen source to the patient, wherein the variable dose is at least partially determined based on the measured blood oxygen content level;

determining if the measured blood oxygen content level is invalid; and

delivering a default amount of oxygen to the patient if the measured blood oxygen content level is invalid.

7. A method according to claim 6, wherein the variable dose of oxygen is at least partially based on a trend in measured blood oxygen content as measured at different times.

8. A method according to claim 6, wherein the variable dose of oxygen is at least partially based on a difference between a desired value for the measured blood oxygen content and the measured blood oxygen content, and wherein the method further comprises changing the desired value for the measured blood oxygen content level.

9. A method according to claim 8, wherein changing the desired value for the measured blood oxygen content level comprises monitoring the patient's heart rate and changing the desired value for the measured blood oxygen content level in response to change in the patient's heart rate.

10. A method according to claim 6, wherein the variable dose includes a zero dose.

11. A method according to claim 6, wherein the oxygen is delivered through a nasal cannula.

12. A method according to claim 6, further comprising determining when the patient is inhaling.

13. A method according to claim 6, further comprising providing an alarm if the measured blood oxygen content level is invalid.

14. A method according to claim 6, further comprising providing an alarm if the patient experiences hypoxemia.

15. A method of controlling oxygen delivery comprising:

continuously measuring blood oxygen content of a patient to obtain a measured blood oxygen content level;

delivering a variable dose of oxygen from an oxygen source to the patient, wherein the variable dose is at least partially determined based on the measured blood oxygen content level;

determining if the measured blood oxygen content level is invalid; and

replacing the invalid measured blood oxygen content level with a value based on a recent trend in blood oxygen content level.

16. A method according to claim 15, wherein the variable dose of oxygen is at least partially based on a trend in measured blood oxygen content as measured at different times.

17. A method according to claim 15, wherein the variable dose of oxygen is at least partially based on a difference between a desired value for the measured blood oxygen content and the measured blood oxygen content, and wherein the method further comprises changing the desired value for the measured blood oxygen content level.

18. A method according to claim 17, wherein changing the desired value for the measured blood oxygen content level comprises monitoring the patient's heart rate and changing the desired value for the measured blood oxygen content level in response to change in the patient's heart rate.

19. A method according to claim 15, wherein the variable dose includes a zero dose.

20. A method according to claim 15, wherein the oxygen is delivered through a nasal cannula.

21. A method according to claim 15, further comprising determining when the patient is inhaling.

22. A method according to claim 15, further comprising providing an alarm if the measured blood oxygen content level is invalid.

23. A method according to claim 15, further comprising providing an alarm if the patient experiences hypoxemia.

24. A system for delivering respiratory oxygen to a patient, the system comprising:

a blood oxygen content level sensor;

a oxygen source;

a valve in fluid communication with the oxygen source;

a controller capable of operating the valve, the controller restricting oxygen flow through the valve when the blood oxygen content level measured by the blood oxygen content level sensor is above a desired value; and

means for determining when the blood oxygen content level measured by the blood oxygen content level sensor is invalid, wherein the controller operates the valve to deliver a default amount of oxygen to the patient when the measured blood oxygen content is invalid.

25. A system according to claim 24, further comprising means for determining when the blood oxygen content level measured by the blood oxygen content level sensor is valid after being invalid, wherein the controller operates the valve to restrict oxygen flow through the valve when the blood oxygen content level measured by the blood oxygen content level sensor is above a desired value.

26. A system according to claim 24, wherein the controller variably restricts oxygen flow through the valve to deliver a variable dose of oxygen from the oxygen source to the patient, wherein the variable dose of oxygen is at least partially determined based on the measured blood oxygen content.

27. A system according to claim 24, wherein the controller determines the variable dose of oxygen at least partially based on a difference between a desired value for the measured blood oxygen content level and the measured blood oxygen content level.

28. A system according to claim 24, wherein the controller determines the variable dose of oxygen at least partially based on a trend in measured blood oxygen content level as measured at different times.

* * * * *