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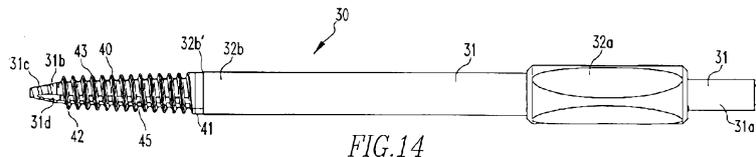


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(57) Abstract: The present disclosure relates to a delivery device. The delivery device including a handle assembly (11), the assembly including a handle (11a) and a connector (11b) coupled to the handle, the connector including a channel (11b') and an opening to the channel; and a shaft (12) coupled to the handle, the shaft including a proximal end and a distal end, the distal end including threads (12c), grooves (12d) intersecting the threads, and a depth stop (12e). Other delivery devices, screws, and delivery device/screw combinations are also disclosed.

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COMPOSITE INTERFERENCE SCREWS AND DRIVERS

[0001] This application is a PCT patent application claiming priority to US Patent Application Serial No. 61/312291, US Patent Application Serial No. 61/334808, and US Patent Application Serial No. 61/359080, the disclosures of which are incorporated herein by reference in their entireties.

[0002] The present disclosure relates to medical apparatuses and procedures in general, and more particularly to medical apparatuses and procedures for reconstructing a ligament.

[0003] In many cases, ligaments are torn or ruptured as the result of an accident. Accordingly, various procedures have been developed to repair or replace such damaged ligaments.

[0004] For example, in the human knee, the anterior and posterior cruciate ligaments (i.e., the "ACL" and "PCL") extend between the top end of the tibia and the bottom end of the femur. Often, the anterior cruciate ligament (i.e., the ACL) is ruptured or torn as the result of, for example, a sports-related injury. Consequently, various surgical procedures have been developed for reconstructing the ACL so as to restore substantially normal function to the knee.

[0005] In many instances, the ACL may be reconstructed by replacing the ruptured ACL with a graft ligament. More particularly, in such a procedure, bone tunnels are generally formed in both the top of the tibia and the bottom of the femur, with one end of the graft ligament being positioned in the femoral tunnel and the other end of the graft ligament being positioned in the

tibial tunnel, and with the intermediate portion of the graft ligament spanning the distance between the bottom of the femur and the top of the tibia. The two ends of the graft ligament are anchored in their respective bone tunnels in various ways well known in the art so that the graft ligament extends between the bottom end of the femur and the top end of the tibia in substantially the same way, and with substantially the same function, as the original ACL. This graft ligament then cooperates with the surrounding anatomical structures so as to restore substantially normal function to the knee.

[0006] In some circumstances, the graft ligament may be a ligament or tendon which is harvested from elsewhere within the patient's body, e.g., a patella tendon with or without bone blocks attached, a semitendinosus tendon and/or a gracilis tendon.

[0007] As noted above, various approaches are well known in the art for anchoring the two ends of the graft ligament in the femoral and tibial bone tunnels.

[0008] In one well-known procedure, which may be applied to femoral fixation, tibial fixation, or both, the end of the graft ligament is placed in the bone tunnel, and then the graft ligament is fixed in place using a headless orthopedic screw, generally known in the art as an "interference" screw. More particularly, with this approach, the end of the graft ligament is placed in the bone tunnel and then the interference screw is advanced into the bone tunnel so that the interference screw extends parallel to the bone tunnel and simultaneously engages both the graft ligament and the side wall of the bone tunnel. In this arrangement, the interference screw essentially drives the graft ligament laterally, into engagement with the opposing side wall of the bone tunnel, whereby to secure the graft ligament to the host bone with a so-called "interference fit". Thereafter, over time (e.g., several months), the graft ligament and the host bone grow

together at their points of contact so as to provide a strong, natural joinder between the ligament and the bone.

[0009] Interference screws have proven to be an effective means for securing a graft ligament in a bone tunnel. However, the interference screw itself generally takes up a substantial amount of space within the bone tunnel, which can limit the surface area contact established between the graft ligament and the side wall of the bone tunnel. This in turn limits the region of bone-to-ligament in-growth, and hence can affect the strength of the joinder. By way of example but not limitation, it has been estimated that the typical interference screw obstructs about 50% of the potential bone-to-ligament integration region.

[0010] For this reason, substantial efforts have been made to provide interference screws fabricated from absorbable materials, so that the interference screw can eventually disappear over time and bone-to-ligament in-growth can take place about the entire perimeter of the bone tunnel. To this end, various absorbable interference screws have been developed which are made from biocompatible, bioabsorbable polymers, e.g., polylactic acid (PLA), polyglycolic acid (PGA), etc. These polymers generally provide the substantial mechanical strength needed to advance the interference screw into position, and to thereafter hold the graft ligament in position while bone-to-ligament in-growth occurs, without remaining in position on a permanent basis.

[0011] In general, interference screws made from such biocompatible, bioabsorbable polymers have proven clinically successful. However, these absorbable interference screws still suffer from several disadvantages. First, clinical evidence suggests that the quality of the bone-to-ligament in-growth is somewhat different than natural bone-to-ligament in-growth, in the sense that the aforementioned bioabsorbable polymers tend to be replaced by a fibrous mass rather than a well-ordered tissue matrix. Second, clinical evidence suggests that absorption

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generally takes a substantial period of time, e.g., on the order of three years or so. Thus, during this absorption time, the bone-to-ligament in-growth is still significantly limited by the presence of the interference screw. Third, clinical evidence suggests that, for many patients, absorption is never complete, leaving a substantial foreign mass remaining within the body. This problem is exacerbated somewhat by the fact that absorbable interference screws generally tend to be fairly large in order to provide them with adequate strength, e.g., it is common for an interference screw to have a diameter (i.e., an outer diameter) of 8-12 mm and a length of 20-25 mm.

[0012] Thus, there is a need for a new and improved interference fixation system which (i) has the strength needed to hold the graft ligament in position while bone-to-ligament in-growth occurs, and (ii) promotes superior bone-to-ligament in-growth.

[0013] In one aspect, the present disclosure relates to a delivery device. The delivery device including a handle assembly, the assembly including a handle and a connector coupled to the handle, the connector including a channel and an opening to the channel; and a shaft coupled to the handle, the shaft including a proximal end and a distal end, the distal end including threads, grooves intersecting the threads, and a depth stop.

[0014] The invention provides an interference screw comprising a proximal end and a distal end, the screw including threads extending in an open helical form from the proximal end to the distal end, a depth stop extending a partial length of the screw from a distal terminal end, and a plurality of runners extending longitudinally along an interior of the screw, wherein the depth stop of the screw is configured to engage a depth stop of a delivery device such that a distal end of the delivery device extends beyond the distal end of the screw.

[0015] The invention also provides a delivery device and screw combination comprising: a delivery device comprising a handle assembly, the assembly including a handle and a connector coupled to the handle, the connector including a channel and an opening to the channel; and a shaft coupled to the handle, the shaft including a proximal end and a distal end, the distal end including threads, grooves intersecting the threads, and a depth stop; and an interference screw coupled to the delivery device comprising a proximal end and a distal end,

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the screw including threads extending in an open helical form from the proximal end to the distal end, a depth stop extending a partial length of the screw from a distal terminal end, and a plurality of runners extending longitudinally along an interior of the screw, the screw located on the distal end of the delivery device such that a proximal end of the depth stop of the screw engages the depth stop of the delivery device and the distal end of the delivery device extends beyond the distal end of the screw.

[0015A] The invention also provides a method for assembling a combination of a delivery device and a screw, the method comprising: inserting a distal end of a delivery device into an opening defined by a proximal end of a screw, the distal end of the delivery device including threads, grooves intersecting the threads, and a depth stop, the screw including threads extending in an open helical form from the proximal end of the screw to a distal end of the screw; and engaging a plurality of runners extending longitudinally along an interior of the screw with the grooves of the delivery device; and engaging a depth stop of the screw, which extends a partial length of the screw from a distal terminal end, with the depth stop of the delivery device such that the distal end of the delivery device extends beyond the distal end of the screw.

[0016] Further areas of applicability of the present disclosure will become apparent from the detailed description provided hereinafter. It should be understood that the detailed description and specific examples, while indicating the preferred embodiment of the disclosure, are intended for purposes of illustration only and are not intended to limit the scope of the disclosure.

[0017] The present invention will now be described, by way of non-limiting example only, with reference to the accompanying drawings, in which:

[0018] Fig. 1 shows a first embodiment of the delivery device of the present disclosure.

[0019] Fig. 2 shows a side view of the shaft of the delivery device of Fig. 1.

[0020] Fig. 2A shows an exploded view of the distal end of the shaft of Fig. 2.

[0021] Fig. 3 shows a cross-sectional view of the shaft of Fig. 2.

[0022] Fig. 4 shows a front view of the distal end of the shaft of Fig. 2.

[0023] Fig. 5 shows an isometric view of the screw for use with the shaft of Fig. 2.

[0024] Fig. 6 shows a side view of the screw of Fig. 5.

[0025] Fig. 7 shows a cross-sectional view of the screw of Fig. 6.

[0026] Fig. 8 shows a second embodiment of a shaft of the present disclosure.

[0027] Fig. 9 shows a side view of the inner member of the shaft of Fig. 8.

[0028] Fig. 9A shows an exploded view of the distal end of the inner member of Fig. 9.

[0029] Fig. 10 shows a cross-sectional view of the inner member of the shaft of Fig. 9.

[0030] Fig. 11 shows a front view of the distal end of the inner member of Fig. 9.

[0031] Fig. 12 shows an isometric view of the outer member of the shaft of Fig. 8.

[0032] Fig. 13 shows a cross-sectional view of the outer member of Fig. 12.

[0033] Figs. 14 and 15 show side views of the shaft of Fig. 8 with the outer member in different positions.

[0034] Fig. 16 shows an isometric view of a third embodiment of a shaft of the present disclosure and a screw for use with the shaft.

[0035] Fig. 17 shows an isometric view of the shaft of Fig. 16.

[0036] Fig. 18 shows an isometric view of the screw of Fig. 16.

[0037] Fig. 19 shows a side view of the screw of Fig. 16.

[0038] Fig. 20 shows a cross-sectional view of the screw of Fig. 19.

[0039] Fig. 21 shows an isometric view of a fourth embodiment of a shaft of the present disclosure and a screw for use with the shaft.

[0040] Fig. 22 shows an isometric view of the screw of Fig. 21.

[0041] Fig. 23 shows an isometric view of the shaft of Fig. 21.

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[0042] Fig. 24 shows an isometric view of the shaft of Fig. 21 and an alternative screw for use with the shaft.

[0043] Fig. 25 shows a side view of the screw of Fig. 24.

[0044] Fig. 26 shows a cross-sectional view of the screw of Fig. 24.

[0045] The following description of the preferred embodiment(s) is merely exemplary in nature and is in no way intended to limit the disclosure, its application, or uses.

[0046] Fig. 1 shows a first embodiment of the delivery device 10 of the present disclosure. The device 10 includes a handle assembly 11 and a shaft 12 coupled to the handle assembly 11. The handle assembly 11 includes a handle 11a and a connector 11b coupled to the handle 11a. The connector 11b has a channel 11b' and an opening 11b'' to the channel 11b'. The opening 11b'' is in the shape of a "D". A proximal end 12a of the shaft 12 is disposed within the channel 11b'.

[0047] Figs. 2, 2A, and 3-4 show the shaft 12. The shaft 12 includes a proximal end 12a and a distal end 12b. The proximal end 12a is in the shape of a "D" to match the shape of the opening 11b''. The distal end 12b includes threads 12c, grooves 12d, and a depth stop 12e. The grooves 12d extend a partial length of the shaft 12 and intersect the threads 12c. The depth stop 12e is for use with a depth stop on a screw that the device 10 is used to implant into a bone tunnel during ligament reconstruction surgery.

[0048] Figs. 5-7 show the screw 20 for use with the delivery device 10 of the present disclosure. The screw 20 includes a proximal end 21 and a distal end 22. A majority of the screw 20 includes screw threads 23 in the form of an open helical coil, i.e. a connected series of continuous regularly spaced turns extending in a helical or spiral form substantially from the

proximal end **21** to the distal end **22** with apertures **24** being defined by the space between the turns of the coil. In other words, interference screw **20** may include an open helical coil defining an internal volume, with the internal volume communicating with the region exterior to the open helical coil through the spacing between the turns of the open helical coil. The distal end **22** also includes a depth stop **25** that extends a partial length of the screw **20**. The depth stop **25** includes a proximal end **25a** and a distal end **25b**. Additionally, a plurality of longitudinally-extending runners **26** extend along the interior of the screw threads **23**.

[0049] The distal end **12b** of the shaft **12** is placed within the interior of the screw **20**, via the opening **27**, until the proximal end **25a** of the depth stop **25** engages the depth stop **12e** of the shaft **12**. During insertion of the shaft **12** into the screw **20**, the runners **26** engage the grooves **12d** and become housed within the grooves **12d**. As shown in Fig. 1, the distal end **12b** of the shaft **12** also includes hash marks **12f**, each of which is associated with a number **12g**. Once the screw **20** is placed on the shaft **12**, the proximal end **21** of the screw **20** aligns with one of the hash marks/numbers **12f**, thereby indicating the length of the screw **20**.

[0050] Figs. 8, 9-9A, and 10-15 show an alternative shaft **30** of the present disclosure. The shaft **30** includes an inner member **31** and an outer member **32** disposed over the inner member **31**. The proximal end **31a** of the inner member **31** is similar in shape to the proximal end **12a** of the shaft **12**. The distal end **31b** of the inner member **31** includes threads **31c**. Grooves **31d** extend along the member **31** and intersect the threads **31c**. Additionally, threads **31e** are located between the proximal and distal ends **31a,31b** of the member **31**. The outer member **32** includes a first section **32a** and a second section **32b**. The first section **32a** has a larger diameter than the second section **32b**. The first section **32a** also includes threads **32c** on an inner wall **32d** of the outer member **32**.

[0051] Once the outer member **32** is disposed over the inner member **31**, threads **32c** engage threads **31e** to move the outer member **32** relative to the inner member **31**. Moving the outer member **32** relative to the inner member **31** allows for more or less of the distal end **31b** of the inner member **31** to be shown. Similar to the distal end **12b** of the shaft **12**, the distal end **31b** of inner member **31** includes hash marks/numbers (**not shown**) that align with an end **32b'** of the second section **32b**, thereby indicating a length of screw **40** that will be disposed on the distal end **31b** of the inner member **31**. As shown in Figs. 14 and 15, the outer member **32** is located at different positions along the length of the inner member **31** to allow for screws **40** of different lengths to be loaded on the distal end **31b** of the inner member **31**.

[0052] A handle assembly, similar to the handle assembly **11**, is coupled to the proximal end **31a** of the inner member **31**. Similar to screw **20**, screw **40** includes a proximal end **41** and a distal end **42**. The screw **40** includes screw threads **43** in the form of an open helical coil having an interior and a plurality of longitudinally-extending runners **45** extending along the interior of the screw threads **43**. Screw **40** is more fully described in United States Patent Application Publication No. 20080154314, the disclosure of which is incorporated herein by reference in its entirety. Once the outer member **32** has been moved to indicate the screw length, the screw **40** is loaded onto the distal end **31b**, such that a proximal end **41** of the screw **40** engages the end **32b'** and the runners **45** engage the grooves **31d** and become housed within the grooves **31d**.

[0053] Figs. 16-20 show another alternative embodiment of the shaft **50** and screw **60** of the present disclosure. The shaft **50** includes a first portion **51** including a proximal end **51a** and a distal end **51b** and a second portion **52** including a first area **52a** and a second area **52b**. The proximal end **51a** is configured to be coupled to a handle assembly, similar to the handle assembly **11**. However, other handle assemblies may be used. The first area **52a** has a smaller

diameter than the first portion **51**, such that a first depth stop **51b'** exists at the distal end **51b** of the first portion **51**. The second area **52b** has a smaller diameter than the first area **52a** such that a second depth stop **52c** exists between the first area **52a** and the second area **52b**. An end **52b'** of the second area **52b** is tapered to allow for easier insertion of the anchor **60** into a bone during ligament reconstruction surgery, as will be further described below. The second portion **52** also includes grooves **53** extending between the first and second areas **52a,52b**. For the purposes of this disclosure, there are three grooves **53**. However, the second portion **52** may include a higher or lower number of grooves **53**.

[0054] Similar to screw **20** shown in Figs. 5-7, screw **60** includes a proximal end **61** and a distal end **62**. A majority of the screw **60** includes screw threads **63** in the form of an open helical coil, i.e. a connected series of continuous regularly spaced turns extending in a helical or spiral form substantially from the proximal end **61** to the distal end **62** with apertures **64** being defined by the space between the turns of the coil. In other words, interference screw **60** may include an open helical coil defining an internal volume, with the internal volume communicating with the region exterior to the open helical coil through the spacing between the turns of the open helical coil. The distal end **62** also includes a depth stop **65** that extends a partial length of the screw **60**. The depth stop **65** includes a proximal end **65a** and a distal end **65b**. Unlike the open depth stop **25** of screw **20** most clearly shown in Fig. 5, the depth stop **65** of screw **60** is a closed depth stop, most clearly shown in Fig. 18. Additionally, a plurality of longitudinally-extending runners **66** extend along the interior of the screw threads **63**.

[0055] The second portion **52** of the shaft **50** is placed within the interior of the screw **60**, via the opening **67**, until the proximal end **65a** of the depth stop **65** engages the second depth stop **52c** of the shaft **50**. During insertion of the shaft **50** into the screw **60**, the runners **66**

engage the grooves **53** and become housed within the grooves **53**. The screws **60** may be of a variety of lengths. For example, a screw **60** may be of such length that its proximal end **61** would engage the first depth stop **51b'**.

[0056] As described above, during ligament reconstruction surgery, the end of the graft ligament is placed in the bone tunnel and then the interference screw **20,40,60** is advanced into the bone tunnel via the use of shafts **12,30,50** so that the interference screw **20,40,60** extends parallel to the bone tunnel and simultaneously engages both the graft ligament and the side wall of the bone tunnel. The screws **20,40,60** may be used in either the femoral or tibial tunnels. Methods of ligament reconstruction via use of the screws **20,40,60** is further shown in the '314 publication shown above.

[0057] Figs. 21-23 show yet another alternative embodiment of the screw **100** and the delivery device **200** of the present disclosure. The screw **100** includes a proximal end **101** and a distal end **102**. A majority of the screw **100** includes screw threads **103** in the form of an open helical coil, i.e. a connected series of continuous regularly spaced turns extending in a helical or spiral form substantially from the proximal end **101** to the distal end **102** with apertures **104** being defined by the space between the turns of the coil. In other words, interference screw **100** may include an open helical coil defining an internal volume, with the internal volume communicating with the region exterior to the open helical coil through the spacing between the turns of the open helical coil. The distal end **102** also includes a suture bridge **105** that extends a partial length of the screw **100**. The suture bridge **105** includes a proximal end **105a** and a distal end **105b**. The distal end **105b** includes a concave shape. A flexible member **110**, such as a suture, is housed within the screw **100**, such that the suture **110** extends around the distal end **105b** of the bridge **105**. Additionally, longitudinally-extending runners **106** extend from the

suture bridge 105 and along the interior of the screw threads 103. For the purposes of this disclosure, there are two longitudinally extending runners 106. However, more or less than two runners are within the scope of this disclosure.

[0058] The delivery device 200 includes a distal end 201 having a slot 202 and grooves 203 extending from the slot 202 on each side of the device 200. As shown in Fig. 21, the screw 100 is located on the distal end 201 such that the suture bridge 105 is housed within the slot 202 and the runners 106 are housed within the grooves 203. The delivery device 200 is cannulated, such that when the screw 100 is located on the device 200, the suture ends 110a,110b extend through the cannulation 204.

[0059] Figs. 24-26 show a screw 300 similar to screw 100. However, screw 300 additionally includes a pointed tip 311 located on the distal end 302. The tip 311 includes a through hole 312. The hole 312 helps in locating the suture 110 within the interior of the screw 300. As shown in Fig. 24, the screw 300 is located on the distal end 201 of delivery device 200 such that the suture bridge 305 is housed within the slot 202 and the runners 306 are housed within the grooves 203. As stated above, the delivery device 200 is cannulated, such that when the screw 300 is located on the device 200, the suture ends 110a,110b extend through the cannulation 204, as shown in Fig. 24.

[0060] For clarity purposes, only the distal end 201 of the device 200 is shown. However, the device 200 would include a proximal end, similar to the devices above, which may be coupled to a handle assembly, similar to handle assembly 11 above. The screws 100,300 are used in the repair of soft tissue, specifically to re-attach tissue to bone. One example of this repair is when the screw 100,300 is delivered into bone via the use of device 200, the device 200 is removed from screw 100,300, the tissue is placed on the bone to be adjacent the screw

100,300, the suture ends 110a,110b are pulled through the tissue, and then the suture ends 110a,110b are tied. A hole may be made in the bone prior to insertion of the screw 100,300 into the bone. However, screw 300 may be inserted into bone without first making a hole in the bone. In this case, the pointed tip 311 is used to start insertion of the screw 300 into the bone and then rotary motion may be used to complete insertion of the screw 300 into the bone. Other methods of tissue repair via use of these screws and delivery device may also be used.

[0061] The handle 11a of handle assembly 11 is made from plastic, however, other non-metal and metal materials may also be used. The shape and size of handle 11a may be any shape and size necessary to help facilitate insertion of the screw 20 into bone. The coupler 11b is made from a metal material, such as stainless steel or titanium, but may be made from other metal and non-metal materials that are strong enough to withstand the forces applied during surgery. The coupler 11b is press-fit to the handle 11a, but may be coupled to the handle 11a in any other manner known to those of skill in the art. The size and shape of the coupler 11b may be any size and shape necessary to help facilitate insertion of the screw 20 into bone. The channel 11b' may be any length necessary and the opening 11b'' may be any shape necessary to facilitate coupling of the shaft 12 to the coupler 11b.

[0062] The shaft 12 is made from a metal material, such as stainless steel and titanium, however, other metal and non-metal materials that would withstand the forces applied during surgery may be used. The diameter of the shaft 12 may vary. The proximal end 12a of the shaft 12 may be any shape necessary to facilitate insertion of the end 12a through opening 11b'' and into channel 11b'. The number of threads 12c and grooves 12d may vary and the lengths of the grooves 12d may also vary. The location of depth stop 12e may also vary based on the diameter

of the shaft **12** and the diameter of the screw **20** that is used. The grooves **12d**, depth stop **12e**, and threads **12c** may be formed by any method known to one of skill in the art.

[0063] The screw **20** is made from a polymer material via a molding method. However, other material, which would allow the screw **20** to withstand forces applied during surgery, and other methods of making may be used. The depth stop **25** is open ended and doesn't extend the entire inner diameter of the screw **20**. The amount of screw inner diameter that the depth stop **25** covers may vary and the length of the depth stop **25** may vary based on the diameter of the screw. The number and length of the runners **26** may also vary. Once the screw **20** is located on the shaft **12**, the distal end **12b** of the shaft **12** extends from the distal end **22** of the screw **20**. During insertion of the screw **20** into bone, the threads **12c** create threads in the bone, thereby creating a seat for the screw threads **23**, as described more fully in the '314 publication. The amount of the distal end **12b** of the shaft **12** that extends from the distal end **22** of the screw **20** may vary.

[0064] The diameters of the first and second sections **32a,32b** of outer member **32** may vary and the number of threads **32c** may also vary. The number of threads **31c,31e** and grooves **31d** may vary and the lengths of the grooves **31d** may also vary. The inner and outer members **31,32** are made from a metal material, such as stainless steel and titanium, and via a method known to one of skill in the art. However, other materials may also be used. The screw **40** is made from a polymer material via a molding method. However, other material and methods of making may be used. The number and length of the runners **45** may also vary. Once the screw **40** is located on the shaft **30**, the distal end **31b** of the shaft **30** extends from the distal end **42** of the screw **40**. During insertion of the screw **40** into bone, the threads **31c** create threads in the bone, thereby creating a seat for the screw threads **43**, as described more fully in the '314

publication. The amount of the distal end 31b of the shaft 30 extending from the screw 40 may vary.

[0065] The shaft 50 is made from a metal material, such as stainless steel or titanium, but may be made from another metal material or a non-metal material that is strong enough to withstand the force applied to the shaft 50 during surgery. The shaft 50 may be made via a method known to one of skill in the art. The diameters of the first and second portions 51,52 may vary along with the number and lengths of the grooves 53 and the locations of the depth stops 52c,51b' may vary based on the diameter of the screw 60 or other factors. Rather than being tapered, the end 52b' may be designed in another manner to allow easier insertion of the screw 60 into bone. The screw 60 is made from a polymer material via a molding method. However, other material, which would allow the screw to withstand the forces applied during surgery, and other methods of making may be used. The number and length of the runners 66 may also vary. Once the screw 60 is located on the shaft 50, the second portion 52 of the shaft 50 extends from the distal end 62 of the screw 60. The amount of the second portion 52 extending from the screw 60 may vary. Additionally, the length of the depth stop 65 may also vary based on the diameter of the screw 60 or other factors.

[0066] The delivery device 200 is made from a metal material, such as stainless steel or titanium, but may be made from a non-metal material that is strong enough to withstand the forces applied to the device 200 during surgery. The delivery device 200 is made via a method known to one of skill in the art. The screws 100,300 are made from a polymer material and via a molding process, however, other material, which would allow the screw to withstand the forces applied during surgery, and other processes known to one of skill in the art may be used. The suture bridge 105 may have a distal end 105b having a shape other than concave and the length

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of the suture bridge **105**, the slot **202**, and the grooves **203** may vary. The size and the shape of the hole **312** may vary.

[0067] While various embodiments of the present invention have been described above, it should be understood that they have been presented by way of example only, and not by way of limitation. It will be apparent to a person skilled in the relevant art that various changes in form and detail can be made therein without departing from the spirit and scope of the invention. Thus, the present invention should not be limited by any of the above described exemplary embodiments.

[0068] Throughout this specification and the claims which follow, unless the context requires otherwise, the word "comprise", and variations such as "comprises" and "comprising", will be understood to imply the inclusion of a stated integer or step or group of integers or steps but not the exclusion of any other integer or step or group of integers or steps.

[0069] The reference in this specification to any prior publication (or information derived from it), or to any matter which is known, is not, and should not be taken as an acknowledgment or admission or any form of suggestion that that prior publication (or information derived from it) or known matter forms part of the common general knowledge in the field of endeavour to which this specification relates.

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THE CLAIMS DEFINING THE INVENTION ARE AS FOLLOWS:

1. An interference screw comprising a proximal end and a distal end, the screw including threads extending in an open helical form from the proximal end to the distal end, a depth stop extending a partial length of the screw from a distal terminal end, and a plurality of runners extending longitudinally along an interior of the screw, wherein the depth stop of the screw is configured to engage a depth stop of a delivery device such that a distal end of the delivery device extends beyond the distal end of the screw.
2. The interference screw of claim 1 wherein the screw is made from a polymer material.
3. The interference screw of claim 1 or 2 wherein the depth stop is an open depth stop encircling part of the distal end of the screw.
4. The interference screw of any one of the preceding claims wherein the depth stop is a closed depth stop encircling the distal end of the screw.
5. The interference screw of any one of the preceding claims wherein the proximal end of the screw aligns with a hash mark on the distal end of the delivery device and a number associated with the hash mark identifies the length of the screw.
6. The interference screw of any one of the preceding claims wherein each of the plurality of runners has a cross sectional shape based on a semi-circle.
7. The interference screw of any one of the preceding claims wherein the plurality of runners includes three runners.
8. A delivery device and screw combination comprising: a delivery device comprising a handle assembly, the assembly including a handle and a connector coupled to the handle, the connector including a channel and an opening to the channel; and a shaft coupled to the handle, the shaft including a proximal end and a distal end, the distal end including threads, grooves intersecting the threads, and a depth stop; and an interference screw coupled to the delivery device comprising a proximal end and a distal end, the screw including threads extending in an open helical form from the proximal end to the distal end, a depth stop extending a partial length of the screw from a distal terminal end, and a plurality of runners

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extending longitudinally along an interior of the screw, the screw located on the distal end of the delivery device such that a proximal end of the depth stop of the screw engages the depth stop of the delivery device and the distal end of the delivery device extends beyond the distal end of the screw.

9. The delivery device and screw combination of claim 8 wherein the screw is made from a polymer material.

10. The delivery device and screw combination of claim 8 or 9 wherein the depth stop of the screw is an open depth stop encircling part of the distal end of the screw.

11. The delivery device and screw combination of any one of claims 8 to 10 wherein the depth stop of the screw is a closed depth stop encircling the distal end of the screw.

12. The delivery device and screw combination of any one of claims 8 to 11 wherein the distal end of delivery device further includes hash marks and the proximal end of the screw aligns with one of the hash marks and a number associated with the one hash mark identifies the length of the screw.

13. The delivery device and screw combination of any one of claims 8 to 12 wherein each of the plurality of runners has a cross-sectional shape based on a semi-circle, and wherein each of the grooves of the delivery device has a shape that is the inverse of the cross-sectional shape of a runner.

14. The delivery device and screw combination of any one of claims 8 to 13 wherein the plurality of runners includes three runners.

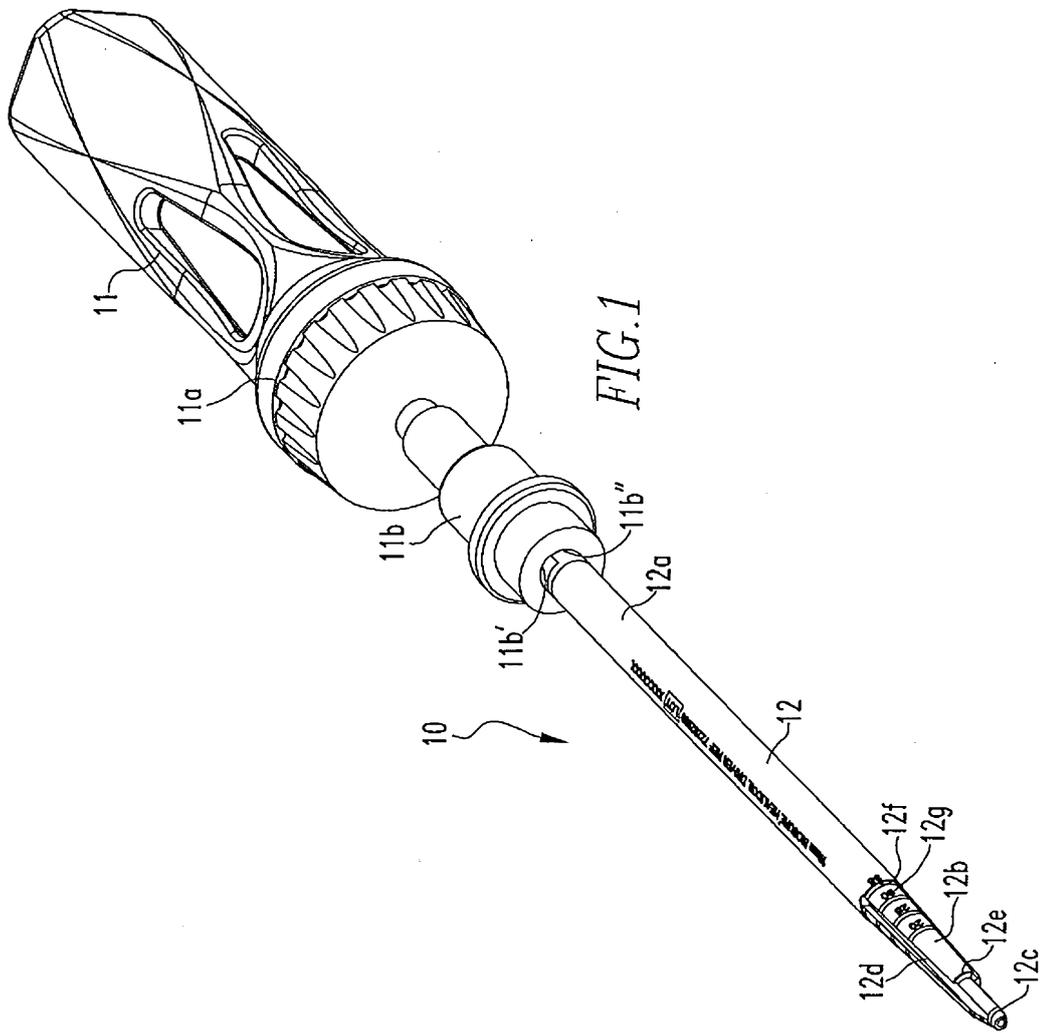
15. The delivery device and screw combination of any one of claims 8 to 14 wherein the delivery device is made from stainless steel or titanium.

16. The delivery device and screw combination of any one of claims 8 to 15 wherein the opening of the connector of the delivery device is in the shape of a "D."

17. A method for assembling a combination of a delivery device and a screw, the method comprising: inserting a distal end of a delivery device into an opening defined by a proximal

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end of a screw, the distal end of the delivery device including threads, grooves intersecting the threads, and a depth stop, the screw including threads extending in an open helical form from the proximal end of the screw to a distal end of the screw; and engaging a plurality of runners extending longitudinally along an interior of the screw with the grooves of the delivery device; and engaging a depth stop of the screw, which extends a partial length of the screw from a distal terminal end, with the depth stop of the delivery device such that the distal end of the delivery device extends beyond the distal end of the screw.



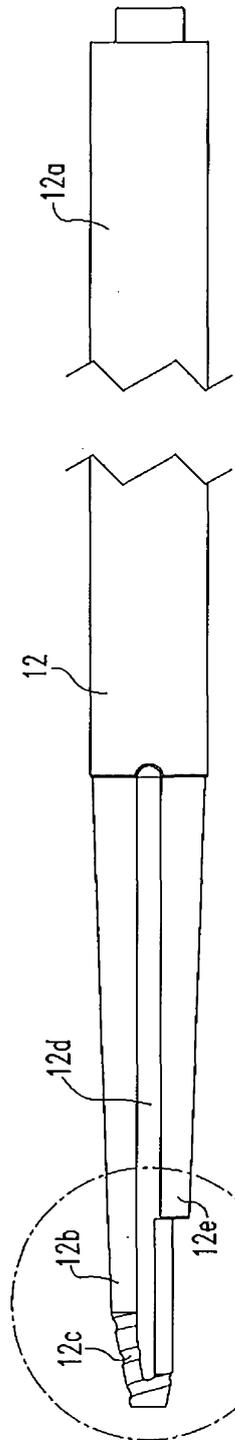


FIG. 2

FIG. 2A

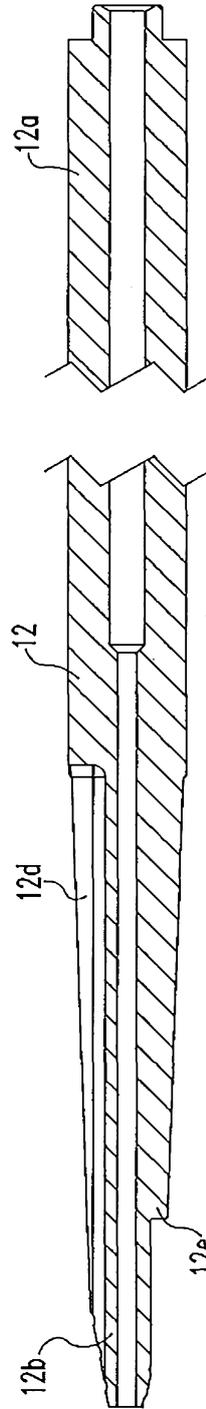


FIG. 3

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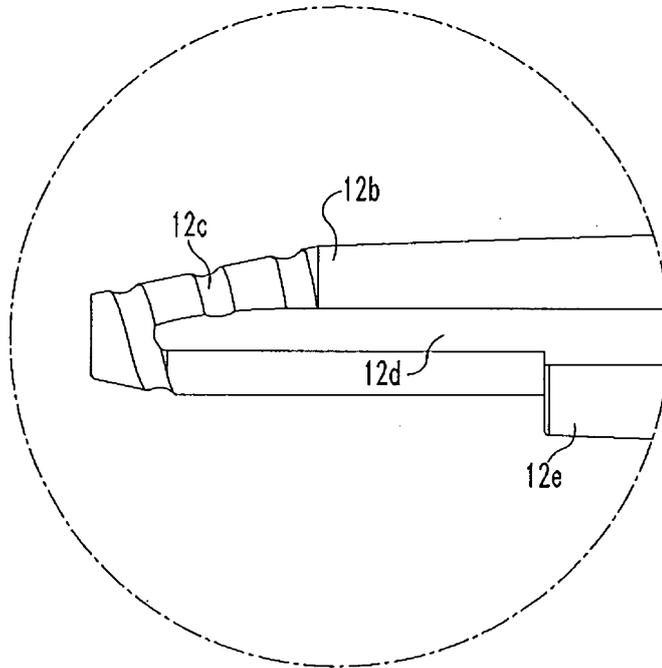


FIG. 2A

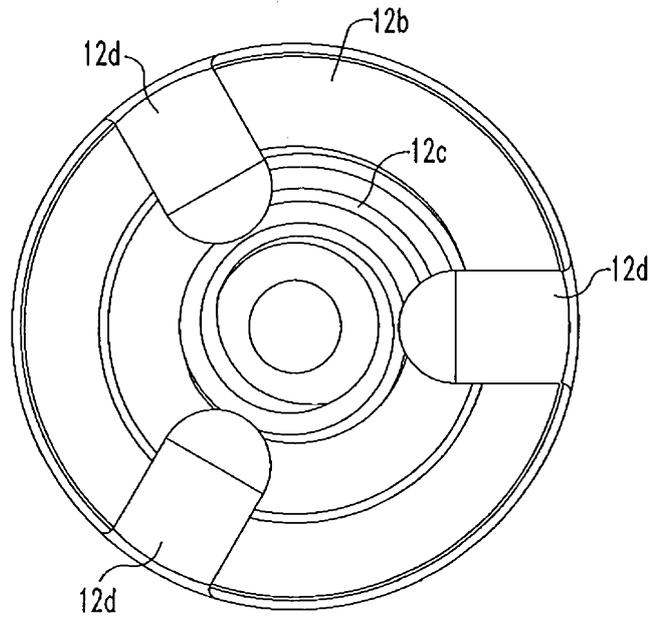
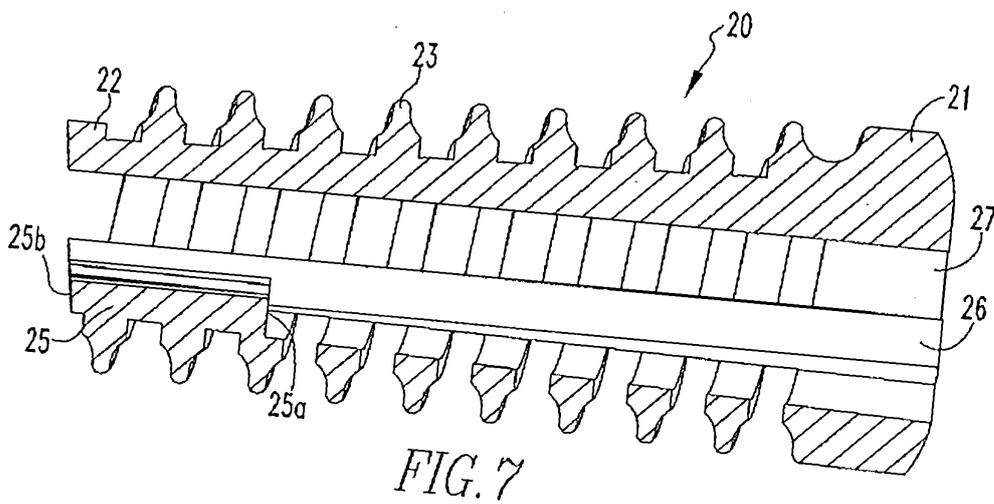
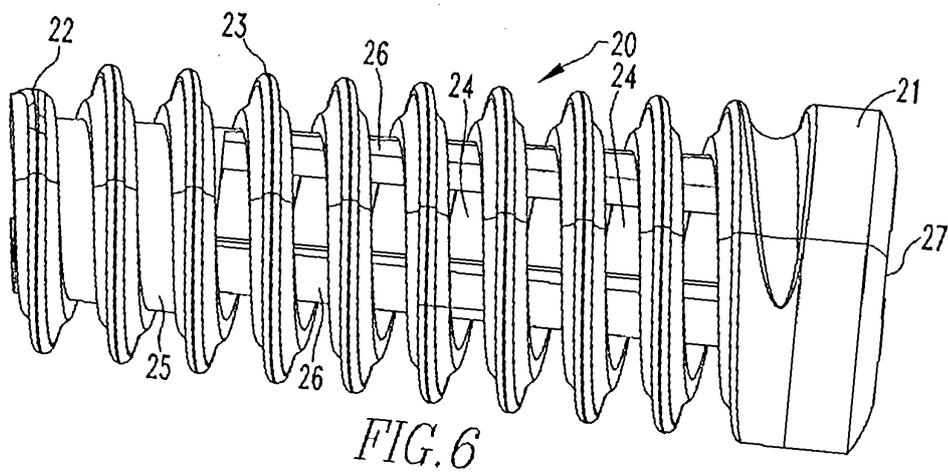
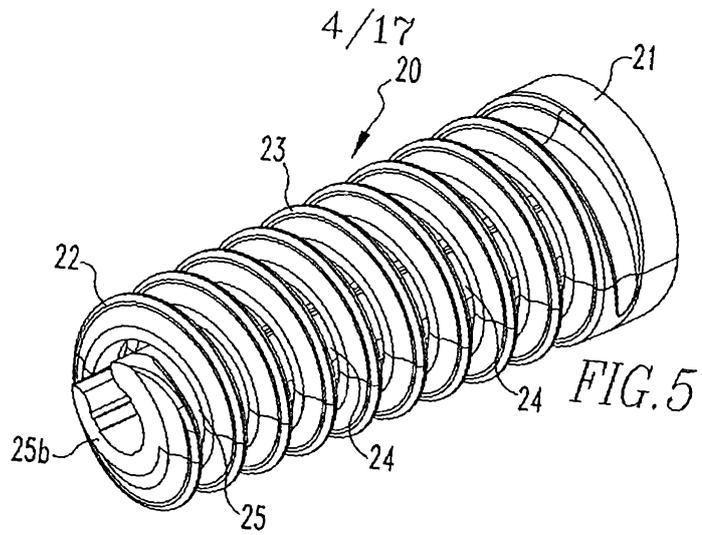
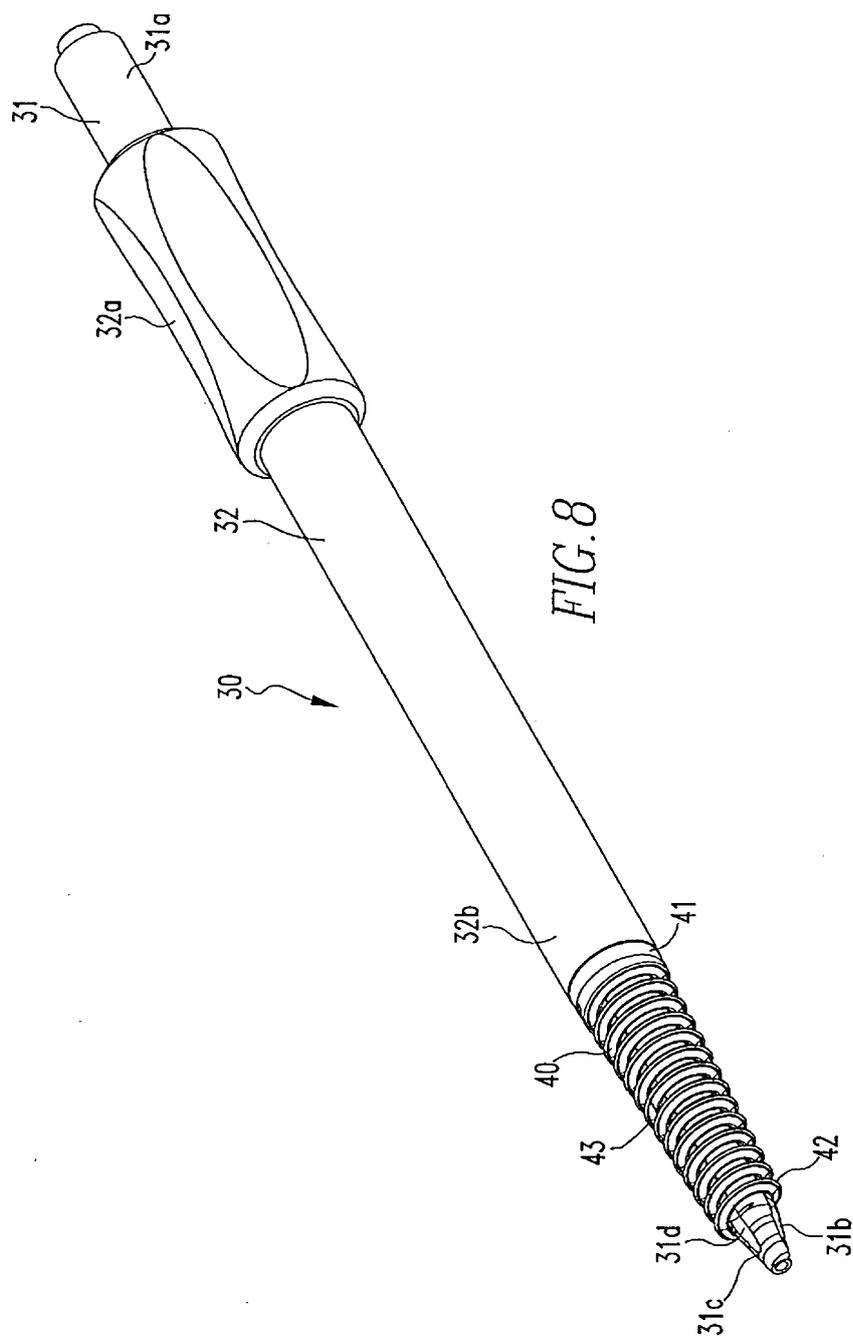
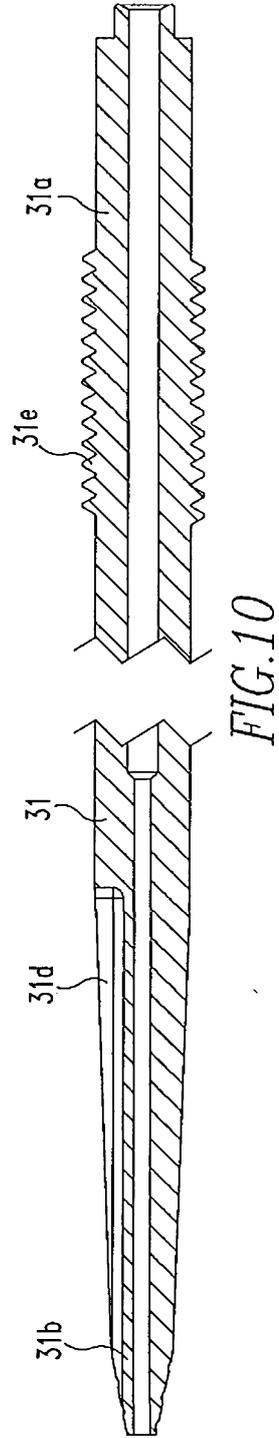
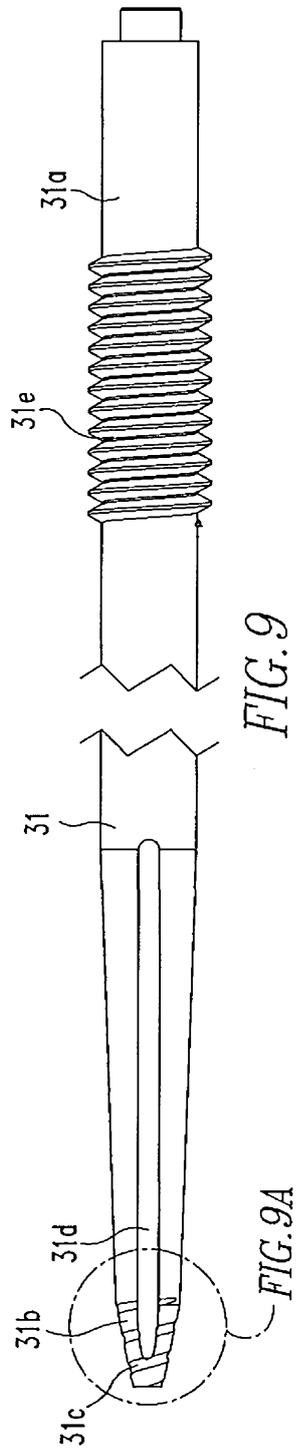


FIG. 4







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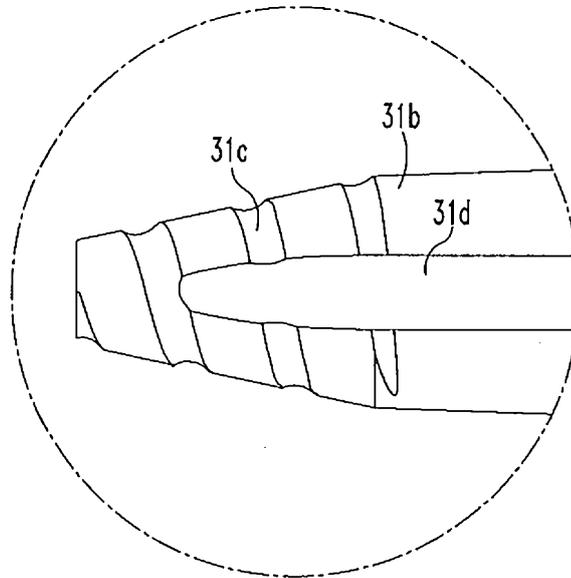


FIG. 9A

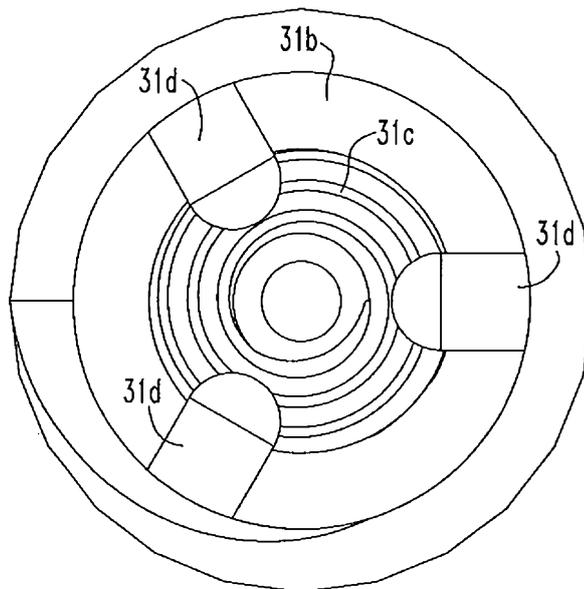


FIG. 11

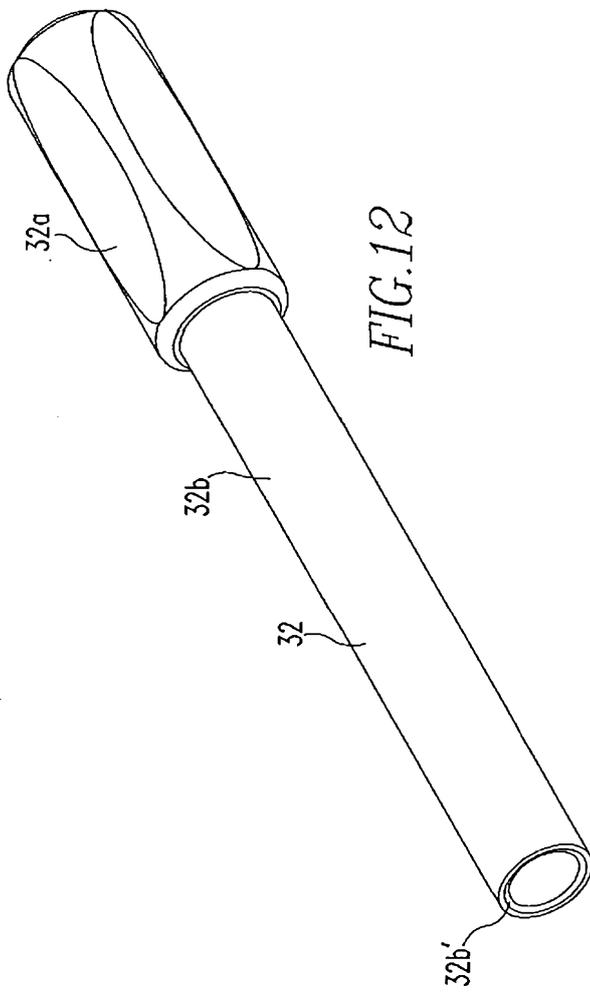


FIG. 12

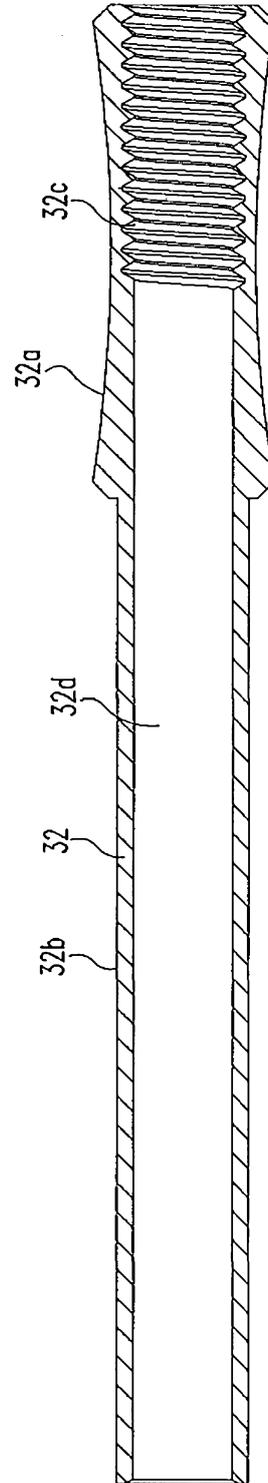
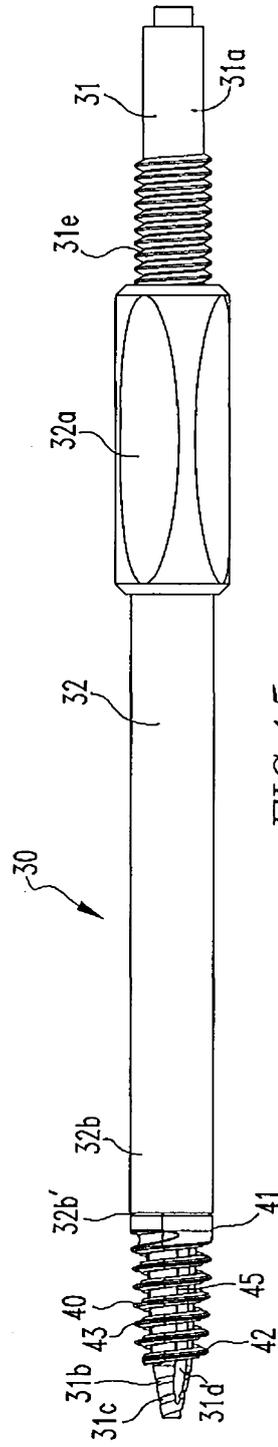
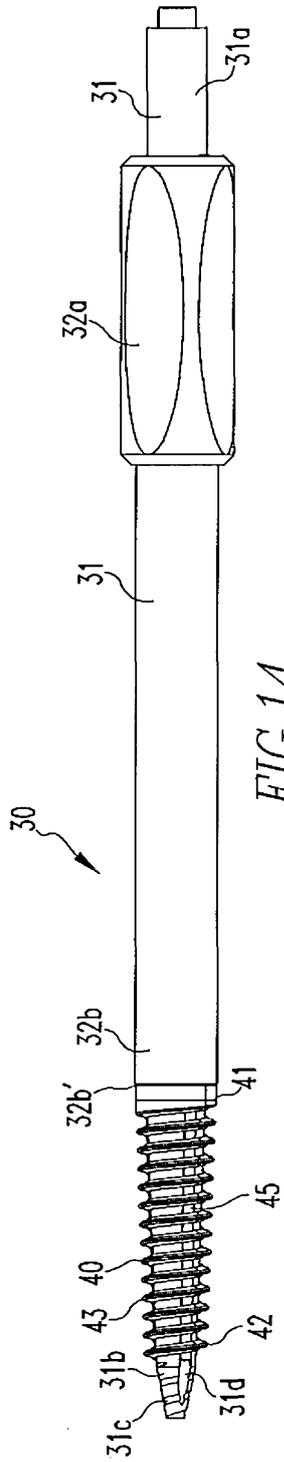


FIG. 13



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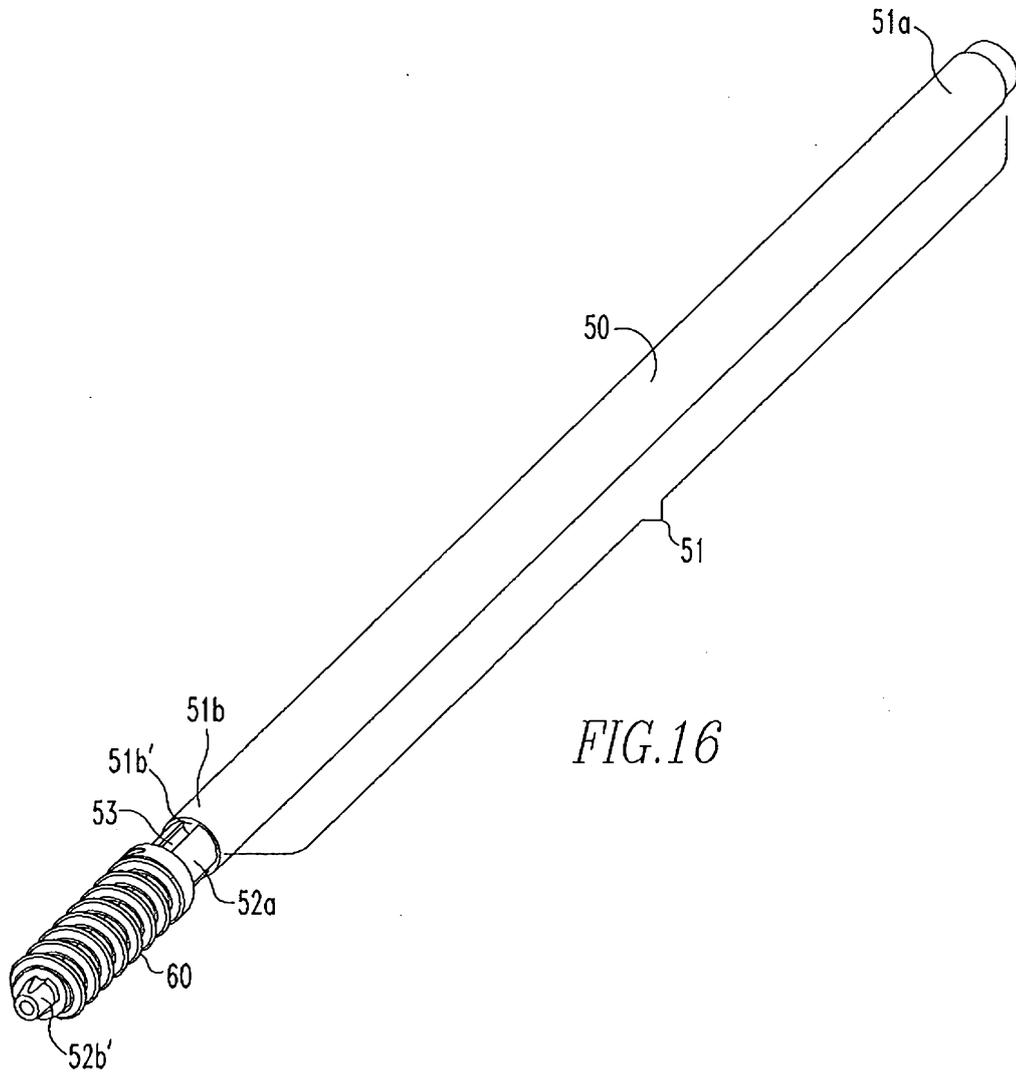


FIG.16

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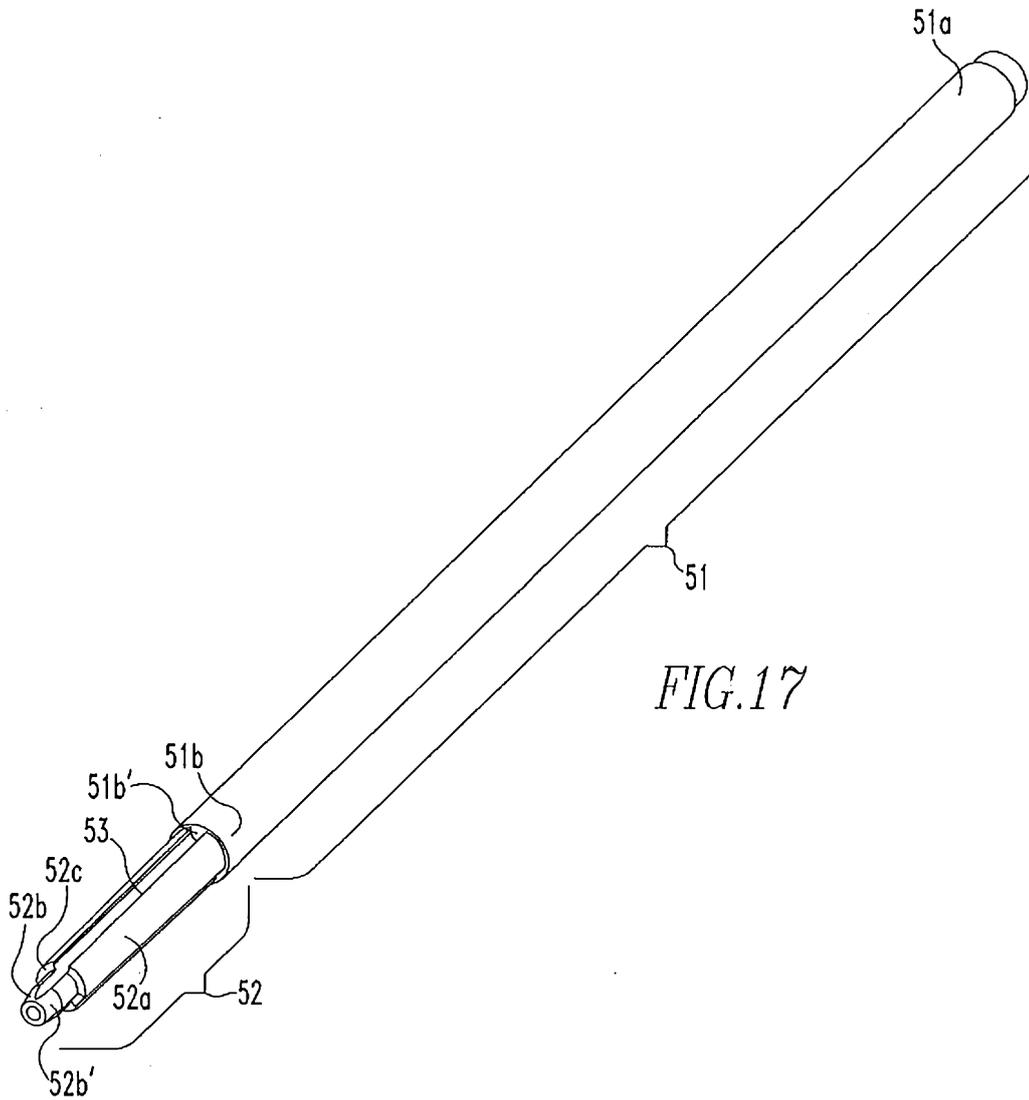
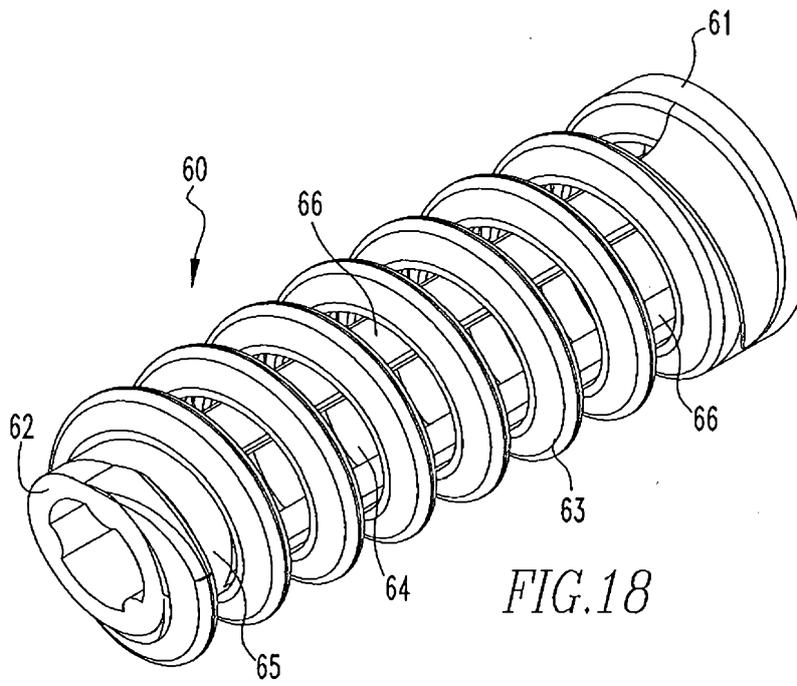
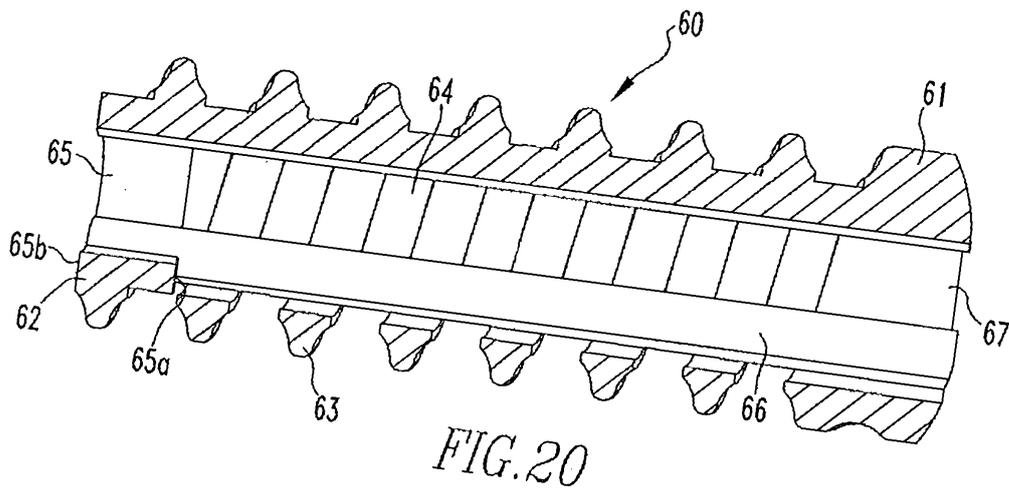
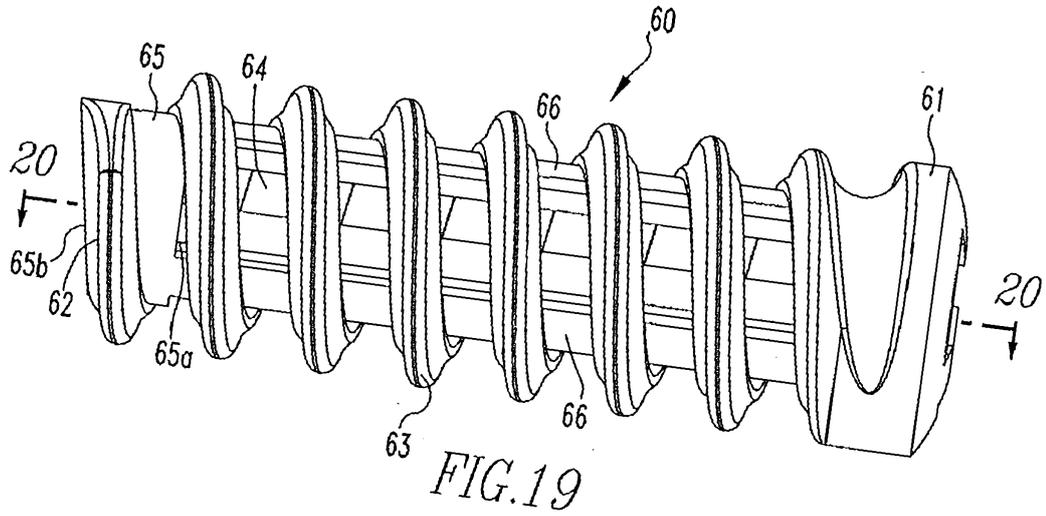


FIG.17



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