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KOVATCHEV B P ET AL: "Symmetrization of the blood glucose measurement scale and its applications", DIABETES, AMERICAN DIABETES ASSOCIATION, ALEXANDRIA, VA, US, vol. 20, no. 11, 1 November 1997 (1997-11-01), pages 1655-1658, XP008128145, ISSN: 0149-5992, DOI: 10.2337/DIACARE.20.11.1655

DESCRIPTION

RELATED APPLICATION

[0001] This application claims priority to U.S. Utility Patent Application Serial No. 15/170,450 filed June 1, 2016 and entitled "CONTROL-TO-RANGE AGGRESSIVENESS".

TECHNICAL FIELD

[0002] The present invention generally relates to processing glucose data measured from a person having diabetes and, in particular, for controlling an adjustment to a basal rate of a therapy delivery device based on the current risk metric and a control-to-range algorithm comprising at least one aggressiveness parameter.

BACKGROUND

[0003] As background, people suffer from either Type I or Type II diabetes in which the sugar level in the blood is not properly regulated by the body. Many of these people may use a continuous glucose monitoring (CGM) to monitor their glucose level on an ongoing basis. In order to perform CGM, a glucose sensor may be placed under the skin which is capable of measuring the glucose level of the person in the interstitial fluid. The glucose sensor may periodically measure the glucose level of the person at a known time interval, such as every one minute, and transmit the results of the glucose measurement result to an insulin pump, blood glucose meter, smart phone or other electronic monitor.

[0004] A system and method for determining a basal rate adjustment based on risk associated with a glucose state of a person with diabetes is disclosed in document US 2015 / 273 147 A1. A method may include detecting a glucose state of the person based on a received glucose measurement signal and determining a current risk metric associated with the detected glucose state. The method may include identifying a reference glucose state and a reference risk metric associated with the reference glucose state, and calculating an adjustment to a basal rate of a therapy delivery device based on the current risk metric associated with the detected glucose state and the reference risk metric associated with the reference glucose level.

[0005] In document US 2014 / 100 435 A1 a system and method is disclosed for analyzing a glucose state. A method may include identifying a target glucose state and an initial glucose state. The method may include calculating a target return path for a transition from the initial glucose state to the target glucose state. The target return path may comprise at least one intermediate glucose state associated with the transition from the initial glucose state to the

target glucose state. The target return path may be calculated based on a hazard associated with the at least one intermediate glucose state of the target return path.

[0006] Document US 2011 / 313 674 A1 discloses embodiments of a testing method for optimizing a therapy to a diabetic patient comprise collecting at least one sampling set of biomarker data, computing a probability distribution function, a hazard function, a risk function, and a risk value for the sampling set of biomarker data, wherein the probability distribution function is calculated to approximate the probability distribution of the biomarker data, the hazard function is a function which yields higher hazard values for biomarker readings in the sampling set indicative of higher risk of complications, the risk function is the product of the probability distribution function and the hazard function, and the risk value is calculated by the integral of the risk function, minimizing the risk value by adjusting the diabetic patient's therapy, and exiting the testing method when the risk value for at least one sampling set is minimized to an optimal risk level.

[0007] The following paper: Kovatchev, B. P. et al., Symmetrization of the blood glucose measurement scale and its applications, Diabetes Care, 1997, 20, 1655-1658 discloses the usage of symmetrized, instead of raw, blood glucose data to strengthen the existing data analysis procedures and allow the development of new statistical techniques.

[0008] In some cases, the measured glucose results (from the glucose sensor) may not accurately represent the glucose concentration. The glucose sensor may malfunction from time to time, such that the measured glucose results (from the glucose sensor) may be substantially different than the actual glucose level of the person. The glucose sensor may malfunction in this manner due to, for example, failure of the sensor electronics or battery or due to sensor "dropout." Sensor dropout may occur due to physiologic problems with the glucose sensor's attachment to the person, such as movement of the sensor relative to the person. Sensor dropout may cause the measured glucose results "drop" to near zero, although the actual glucose level of the person may be much higher. Additionally, the calibration of the glucose sensor may drift resulting in a bias toward greater than the true current blood glucose level or less than the true current blood glucose level. The glucose sensor may also experience an error which causes the CGM to no longer response to changes in the true blood glucose level and remain at an incorrect artificially high or artificially low blood glucose reading. Finally, a glucose sensor may be in the first day of use and have error in blood glucose measurement until stabilization.

[0009] As a result, embodiments of the present disclosure may process the measured glucose results from the person such that the actual glucose level of the person may be estimated, even in the presence of sensor noise and/or sensor malfunction. In addition, the future glucose level of the person may be predicted, based on the estimated glucose level.

[0010] As a result, embodiments of the present disclosure may implement an aggressiveness parameter in adjusting basal insulin rates to account for glucose sensor error.

SUMMARY

[0011] The present invention is defined by the appended claims.

[0012] In one embodiment, a method of determining a basal rate adjustment of insulin in a continuous glucose monitoring system of a person with diabetes is provided. The method includes receiving, by at least one computing device, a signal representative of at least one glucose measurement. Further, the method includes detecting, by the at least one computing device, a glucose state of the person based on the signal, the detected glucose state including a glucose level of the person and a rate of change of the glucose level. Additionally, the method includes determining, by the at least one computing device, a current risk metric, the current risk metric indicating a risk of at least one of a hypoglycemic condition and a hyperglycemic condition of the person. Determining the current risk metric comprises determining, by the at least one computing device, a return path based on a transition from the detected glucose state to a target glucose state, the return path comprising at least one intermediate glucose value associated with a return to the target glucose state; determining, by the at least one computing device, hazard values for a given glucose level of the at least one intermediate glucose value with a hazard function, each hazard value being indicative of a hazard associated with the corresponding intermediate glucose value; determining, by the at least one computing device, a cumulative hazard value of the return path, the cumulative hazard value including a sum of the hazard values of the at least one glucose value on the return path; and determining, by the at least one computing device, a weighted average of cumulative hazard values of return paths generated from a glucose state distribution around the detected glucose state. Finally, the method includes calculating, by the at least one computing device, an adjustment to a basal rate of a therapy delivery device based on the current risk metric and a control-to-range algorithm comprising at least one aggressiveness parameter. The aggressiveness parameter selected from: (a) providing a scaling parameter α_{hyper} comprised by the hazard function to adjust positive hazard values associated with hyperglycemia; (b) providing a shift parameter Δg_{hyper} comprised by the hazard function to shift positive hazard values to account for insulin on board following a meal or correction bolus; (c) adjustment to a maximum allowed glucose acceleration utilized by the return path, glucose acceleration representing the rate of change of glucose velocity and glucose velocity representing the rate of change of glucose values; (d) adjustment to a glucose state uncertainty representing the level of trust in the measured glucose state for weighting the glucose states; or (e) combinations thereof. The hazard value for each of the hazard values of the at least one glucose value on the return path is determined by the at least one computing device in accordance with a hazard function as follows

$$h(g)_{hyper} = \max(\alpha_{hyper} \cdot \alpha(\log(\max(g - \Delta g_{hyper} - \max(\Delta g_{hypo}, 0), 1)))^c - \beta, 0),$$

$$h(g)_{hypo} = \min(\alpha(\log(\max(g - \Delta g_{hypo}, 1)))^c - \beta, 0),$$

and

$$\begin{cases} h_{MAX} & \text{if } g - \Delta g_{hyper} - \max(\Delta g_{hypo}, 0) \geq g_{MAX} \\ \cdot & \cdot \\ \cdot & \cdot \end{cases}$$

$$h(g) = \begin{cases} h_{MIN} & \text{if } g - \Delta g_{hyper} \leq g_{MIN} \\ h(g)_{hyper} & \text{if } h(g)_{hyper} \geq 0 \\ h(g)_{hypo} & \text{if } h(g)_{hypo} < 0 \end{cases}$$

where g is the glucose value, Δg_{hyper} is a hyperglycemic shift to account for a recent meal or correction bolus, Δg_{hypo} is a hypoglycemic shift to account for recent exercise or glucagon, h_{MAX} is a maximum hazard value representing the hazard for a glucose value of 600 mg/dl, g_{MAX} is a glucose value above which no additional incremental hazard is calculated above h_{MAX} , h_{MIN} is a minimum hazard representing the hazard value for a glucose value of 10 mg/dl, g_{MIN} is a glucose value below which no additional incremental hazard is calculated above h_{MIN} , α_{hyper} is the hyperglycemic control aggressiveness to adjust for insulin sensitivity, and α , β , and c are process variables.

[0013] In another embodiment, a blood glucose management device configured to determine a basal rate adjustment in a continuous glucose monitoring system of a person with diabetes is provided. The device includes a non-transitory computer-readable medium storing executable instructions and at least one processing device configured to execute the executable instructions such that, when executed by the at least one processing device, the executable instructions cause the at least one processing device to receive a signal representative of at least one glucose measurement. Additionally, the executable instructions cause the at least one processing device to detect a glucose state of the person based on the signal, the detected glucose state including a glucose level of the person and a rate of change of the glucose level. Further, the executable instructions cause the at least one processing device to determine a current risk metric, the current risk metric indicating a risk of at least one of a hypoglycemic condition and a hyperglycemic condition of a person. Determining the current risk metric comprises determining, by the at least one computing device, a return path based on a transition from the detected glucose state to a target glucose state, the return path comprising at least one intermediate glucose value associated with a return to the target glucose state; determining, by the at least one computing device, hazard values for a given glucose level of the at least one intermediate glucose value with a hazard function, each hazard value being indicative of a hazard associated with the corresponding intermediate glucose value; determining, by the at least one computing device, a cumulative hazard value of the return path, the cumulative hazard value including a sum of the hazard values of the at least one glucose value on the return path; and determining, by the at least one computing device, a weighted average of cumulative hazard values of return paths generated from a glucose state distribution around the detected glucose state. Finally, the executable instructions cause the at least one processing device to calculate an adjustment to a basal rate of a therapy delivery based on the current risk metric and a control-to-range algorithm comprising at least one aggressiveness parameter. The aggressiveness parameter selected from: (a) providing a scaling parameter α_{hyper} comprised by the hazard function to adjust positive hazard values associated with hyperglycemia; (b) providing a shift parameter Δg_{hyper} comprised by the hazard function to shift positive hazard values to account for insulin on board following a meal or correction bolus; (c) adjustment to a maximum allowed glucose acceleration utilized by the return path, glucose acceleration representing the rate of change of

glucose velocity and glucose velocity representing the rate of change of glucose values; (d) adjustment to a glucose state uncertainty representing the level of trust in the measured glucose state for weighting the glucose states; or (e) combinations thereof. The hazard value for each of the hazard values of the at least one glucose value on the return path is determined by the at least one computing device in accordance with a hazard function as follows

$$h(g)_{hyper} = \max(\alpha_{hyper} \cdot \alpha (\log(\max(g - \Delta g_{hyper} - \max(\Delta g_{hypo}, 0), 1)))^c - \beta, 0),$$

$$h(g)_{hypo} = \min(\alpha (\log(\max(g - \Delta g_{hypo}, 1)))^c - \beta, 0),$$

and

$$h(g) = \begin{cases} h_{MAX} & \text{if } g - \Delta g_{hyper} - \max(\Delta g_{hypo}, 0) \geq g_{MAX} \\ h_{MIN} & \text{if } g - \Delta g_{hypo} \leq g_{MIN} \\ h(g)_{hyper} & \text{if } h(g)_{hypo} \geq 0 \\ h(g)_{hypo} & \text{if } h(g)_{hypo} < 0 \end{cases}$$

where g is the glucose value, Δg_{hyper} is a hyperglycemic shift to account for a recent meal or correction bolus, Δg_{hypo} is a hypoglycemic shift to account for recent exercise or glucagon, h_{MAX} is a maximum hazard value representing the hazard for a glucose value of 600 mg/dl, g_{MAX} is a glucose value above which no additional incremental hazard is calculated above h_{MAX} , h_{MIN} is a minimum hazard representing the hazard value for a glucose value of 10 mg/dl, g_{MIN} is a glucose value below which no additional incremental hazard is calculated above h_{MIN} , α_{hyper} is the hyperglycemic control aggressiveness to adjust for insulin sensitivity, and α , β , and c are process variables.

BRIEF DESCRIPTION OF THE DRAWINGS

[0014] The embodiments set forth in the drawings are illustrative and exemplary in nature and not intended to limit the inventions defined by the claims. The following detailed description of the illustrative embodiments can be understood when read in conjunction with the following drawings, where like structure is indicated with like reference numerals and in which:

FIG. 1 illustrates a continuous glucose monitoring (CGM) system according to one or more embodiments shown and described herein;

FIG. 2 illustrates an exemplary blood glucose management device, therapy delivery device, and glucose sensor of the CGM system of FIG. 2, the blood glucose management device including a bolus calculator module, control-to-range logic, and basal rate adjustment logic;

FIG. 3 illustrates a graph plotting an exemplary CGM trace and an adjusted maximum allowed glucose following a meal event;

FIGS. 4A and 4B illustrate typical basal multipliers and basal multipliers with implementation of a risk scaling aggressiveness parameter respectively according to one or more embodiments shown and described herein;

FIG. 4C illustrates a plot of a nominal hazard function and the hazard function with implementation of a hyperglycemic risk scaling and hyperglycemic risk shifting respectively;

FIGS. 5A and 5B illustrate typical basal multipliers and basal multipliers with implementation of a risk shifting aggressiveness parameter respectively according to one or more embodiments shown and described herein;

FIGS. 6A and 6B illustrate typical basal multipliers and basal multipliers with implementation of an increased maximum allowed acceleration aggressiveness parameter respectively according to one or more embodiments shown and described herein;

FIGS. 7A and 7B illustrate typical basal multipliers and basal multipliers with implementation of a decreased maximum allowed aggressiveness parameter respectively according to one or more embodiments shown and described herein;

FIGS. 8A and 8B illustrate typical basal multipliers and basal multipliers with implementation of an increased uncertainty aggressiveness parameter respectively according to one or more embodiments shown and described herein; and

FIGS. 9A and 9B illustrate typical basal multipliers and basal multipliers with implementation of a decreased uncertainty aggressiveness parameter respectively according to one or more embodiments shown and described herein.

DETAILED DESCRIPTION

[0015] The embodiments described herein generally relate to methods and systems for determining a basal rate adjustment of insulin in a continuous glucose monitoring system of a person with diabetes and, in particular, for implementing at least one aggressiveness parameter in determining adjustments to basal rate. For the purposes of defining the present disclosure, the "measured glucose results" are the glucose levels of the person as measured by the glucose sensor; the "actual glucose level" or "true glucose measurement" is the actual glucose level of the person.

[0016] Referring to FIG. 1, an exemplary continuous glucose monitoring (CGM) system **10** is illustrated for monitoring the glucose level of a person with diabetes (PWD) **11**. In particular, CGM system **10** is operative to collect a measured glucose value at a predetermined, adjustable interval, such as every one minute, five minutes, or at other suitable intervals. CGM system **10** illustratively includes a glucose sensor **16** having a needle or probe **18** that is inserted under the skin **12** of the person. The end of the needle **18** is positioned in interstitial fluid **14**, such as blood or another bodily fluid, such that measurements taken by glucose sensor **16** are based on the level of glucose in interstitial fluid **14**. Glucose sensor **16** is positioned adjacent the abdomen of the person or at another suitable location. Furthermore,

the glucose sensor **16** may be periodically calibrated in order to improve its accuracy. This periodic calibration may help correct for sensor drift due to sensor degradation and changes in the physiological condition of the sensor insertion site. Glucose sensor **16** may comprise other components as well, including but not limited to a wireless transmitter **20** and an antenna **22**. Glucose sensor **16** may alternatively use other suitable devices for taking measurements, such as, for example, a non-invasive device (e.g., infrared light sensor). Upon taking a measurement, glucose sensor **16** transmits the measured glucose value via a communication link **24** to a computing device **26**, illustratively a blood glucose (bG) management device **26**. The bG management device **26** may also be configured to store in memory **39** a plurality of measured glucose results received from the glucose sensor **16** over a period of time.

[0017] CGM system **10** further includes a therapy delivery device **31**, illustratively an insulin infusion pump **31**, for delivering therapy (e.g., insulin) to the person. Insulin pump **31** is in communication with management device **26** via a communication link **35**, and management device **26** is able to communicate bolus and basal rate information to insulin pump **31**. Insulin pump **31** includes a catheter **33** having a needle that is inserted through the skin **12** of the person **11** for injecting the insulin. Insulin pump **31** is illustratively positioned adjacent the abdomen of the person or at another suitable location. Similar to glucose sensor **16**, infusion pump **31** also includes a wireless transmitter and an antenna for communication with management device **26**. Insulin pump **31** is operative to deliver basal insulin (e.g., small doses of insulin continuously or repeatedly released at a basal rate) and bolus insulin (e.g., a surge dose of insulin, such as around a meal event, for example). The bolus insulin may be delivered in response to a user input triggered by the user, or in response to a command from management device **26**. Similarly, the basal rate of the basal insulin is set based on user input or in response to a command from management device **26**. Infusion pump **31** may include a display for displaying pump data and a user interface providing user controls. In an alternative embodiment, insulin pump **31** and glucose sensor **16** may be provided as a single device worn by the patient, and at least a portion of the logic provided by processor or microcontroller may reside on this single device. Bolus insulin may also be injected by other means, such as manually by the user via a needle.

[0018] In one embodiment, such a CGM system **10** is referred to as an artificial pancreas system that provides closed loop or semi-closed loop therapy to the patient to approach or mimic the natural functions of a healthy pancreas. In such a system, insulin doses are calculated based on the CGM readings and are automatically delivered to the patient based on the CGM reading. For example, if the CGM indicates that the user has a high blood glucose level or hyperglycemia, the system can calculate an insulin dose necessary to reduce the user's blood glucose level below a threshold level or to a target level and automatically deliver the dose. Alternatively, the system can automatically suggest a change in therapy such as an increased insulin basal rate or delivery of a bolus, but can require the user to accept the suggested change prior to delivery. If the CGM data indicates that the user has a low blood glucose level or hypoglycemia, the system can, for example, automatically reduce a basal rate, suggest to the user to reduce a basal rate, automatically deliver or suggest that the user initiate the delivery of an amount of a substance such as, e.g., a hormone (glucagon) to raise

the concentration of glucose in the blood, suggest that the user, e.g., ingest carbohydrates and/or automatically take other actions and/or make other suggestions as may be appropriate to address the hypoglycemic condition, singly or in any desired combination or sequence. In some embodiments, multiple medicaments can be employed in such a system such as a first medicament, e.g., insulin, that lowers blood glucose levels and a second medicament, e.g., glucagon, which raises blood glucose levels.

[0019] Communication links **24**, **35** are illustratively wireless, such as a radio frequency ("RF") or other suitable wireless frequency, in which data and controls are transmitted via electromagnetic waves between sensor **16**, therapy delivery device **31**, and management device **26**. Bluetooth® is one exemplary type of wireless RF communication system that uses a frequency of approximately 2.4 Gigahertz (GHz). Another exemplary type of wireless communication scheme uses infrared light, such as the systems supported by the Infrared Data Association® (IrDA®). Other suitable types of wireless communication may be provided. Furthermore, each communication link **24**, **35** may facilitate communication between multiple devices, such as between glucose sensor **16**, computing device **26**, insulin pump **31**, and other suitable devices or systems. Wired links may alternatively be provided between devices of system **10**, such as, for example, a wired Ethernet link. Other suitable public or proprietary wired or wireless links may be used.

[0020] FIG. 2 illustrates an exemplary management device **26** of the CGM system **10** of FIG. 2. Management device **26** includes at least one microprocessor or microcontroller **32** that executes software and/or firmware code stored in memory **39** of management device **26**. The software/firmware code contains instructions that, when executed by the microcontroller **32** of management device **26**, causes management device **26** to perform the functions described herein. Management device **26** may alternatively include one or more application-specific integrated circuits (ASICs), field-programmable gate arrays (FPGAs), digital signal processors (DSPs), hardwired logic, or combinations thereof. While management device **26** is illustratively a glucose monitor **26**, other suitable management devices **26** may be provided, such as, for example, desktop computers, laptop computers, computer servers, personal data assistants ("PDA"), smart phones, cellular devices, tablet computers, infusion pumps, an integrated device including a glucose measurement engine and a PDA or cell phone, etc. Although management device **26** is illustrated as a single management device **26**, multiple computing devices may be used together to perform the functions of management device **26** described herein.

[0021] Memory **39** is any suitable computer readable medium that is accessible by microcontroller **32**. Memory **39** may be a single storage device or multiple storage devices, may be located internally or externally to management device **26**, and may include both volatile and non-volatile media. Further, memory **39** may include one or both of removable and non-removable media. Exemplary memory **39** includes random-access memory (RAM), read-only memory (ROM), electrically erasable programmable ROM (EEPROM), flash memory, CD-ROM, Digital Versatile Disk (DVD) or other optical disk storage, a magnetic storage device, or any other suitable medium which is configured to store data and which is accessible by

management device **26**.

[0022] The microcontroller **32** may also include additional programming to allow the microcontroller **32** to learn user preferences and/or user characteristics and/or user history data. This information can be utilized to implement changes in use, suggestions based on detected trends, such as, weight gain or loss. The microcontroller **32** can also include programming that allows the device **26** to generate reports, such as reports based upon user history, compliance, trending, and/or other such data. Additionally insulin infusion pump **31** embodiments of the disclosure may include a "power off" or "suspend" function for suspending one or more functions of the device **26**, such as, suspending a delivery protocol, and/or for powering off the device **26** or the delivery mechanism thereof. For some embodiments, two or more microcontrollers **32** may be used for controller functions of insulin infusion pump **31**, including a high power controller and a low power controller used to maintain programming and pumping functions in low power mode, in order to save battery life.

[0023] Management device **26** further includes a communication device **41** operatively coupled to microcontroller **32**. Communication device **41** includes any suitable wireless and/or wired communication module operative to transmit and receive data and controls over communication links **24**, **35** between device **26** and glucose sensor **16** and insulin pump **31**. In one embodiment, communication device **41** includes an antenna **30** (FIG. 1) for receiving and/or transmitting data wirelessly over communication links **24**, **35**. Management device **26** stores in memory **39** measured glucose results and other data received from glucose sensor **16** and/or insulin pump **31** via communication device **41**.

[0024] Management device **26** includes one or more user input device(s) **34** for receiving user input. Input device(s) **34** may include pushbuttons, switches, a mouse pointer, keyboard, touchscreen, or any other suitable input device. Display **28** is operatively coupled to microcontroller **32**, and may comprise any suitable display or monitor technology (e.g., liquid crystal display, etc.) configured to display information provided by microcontroller **32** to a user. Microcontroller **32** is configured to transmit to display **28** information related to the detected glucose state of the person, the risk associated with the glucose state, and basal rate and bolus information. The glucose state may include the estimated glucose level and the estimated rate-of-change of the glucose level, as well as an estimate of the quality or uncertainty of the estimated glucose level. Moreover, the displayed information may include warnings, alerts, etc. regarding whether the estimated or predicted glucose level of the person is hypoglycemic or hyperglycemic. For example, a warning may be issued if the person's glucose level falls below (or is predicted to fall below) a predetermined hypoglycemic threshold, such as 50 to 70 milligrams of glucose per deciliter of blood (mg/dl). Management device **26** may also be configured to tactilely communicate information or warnings to the person, such as for example by vibrating.

[0025] In one embodiment, management device **26** is in communication with a remote computing device (not shown), such as at a caregiver's facility or a location accessible by a caregiver, and data (e.g., glucose data or other physiological information) is transferred

between them. In this embodiment, management device **26** and the remote device are configured to transfer physiological information through a data connection such as, for example, via the Internet, cellular communications, or the physical transfer of a memory device such as a diskette, USB key, compact disc, or other portable memory device.

[0026] Microcontroller **32** also includes control-to-range logic **44**. A control-to-range system reduces the likelihood of a hypoglycemic event or a hyperglycemic event by adjusting insulin dosing only if the PWD's 11 glucose level approaches the low or high glucose thresholds.

[0027] Microcontroller **32** includes hazard analysis logic **40** that calculates target return paths from a plurality of initial glucose states to a target glucose state based on cumulative hazard values. The target glucose state is illustratively an optimal or ideal glucose state having no associated hazard or risk, such as a glucose level of 112.5 mg/dl and a glucose rate-of-change of zero, although any suitable target glucose state may be identified. Each target return path is comprised of a plurality of intermediate glucose states that are to be encountered during a transition from the initial glucose state to the target glucose state. Cumulative penalty values associated with the target return paths are stored in memory **76** that may be used as a lookup table. Calculation of cumulative penalty values is discussed *infra*.

[0028] In some embodiments, inaccurate glucose measurements may result from malfunction and/or noise associated with glucose sensor **24**. As such, hazard analysis logic **40** analyzes the probability of accuracy of the detected glucose state provided with glucose sensor **24**. Hazard analysis logic **40** may use any suitable probability analysis tool to determine the probability of accuracy of a measured glucose result, such as a hidden Markov model. Based on the determined probability of accuracy, hazard analysis logic **40** estimates the glucose level and the glucose rate of change of the person using a recursive filter **42**. In particular, recursive filter **42**, such as a Kalman filter, for example, weights the detected glucose state, including the glucose level and rate of change, with the determined probability of glucose sensor accuracy. Based on the probability of glucose sensor accuracy, recursive filter **42** calculates an uncertainty measure of the estimated glucose state. The uncertainty measure is indicative of the quality of the estimated glucose state. For a series of detected glucose states, the uncertainty for each state may vary.

[0029] Microcontroller **32** of FIG. 2 further includes a bolus calculator module **48** that calculates bolus recommendations and a maximum allowed glucose level of a user which may be displayed to a user via display **28**. Management device **26** maintains a record in memory **39** of historical data for the user accumulated over time leading up to the current time. The historical data includes blood glucose history, prescription data, prior bolus recommendations, prior administered boluses, prior basal rates, glucose sensitivity factors for the user's sensitivity to insulin and carbohydrates, blood glucose responses to prior boluses and meal events, other user health and medical data, and the time stamp of each event and data recordation. The history data includes patient recorded information such as meal events, amount of carbohydrates consumed, confirmations of bolus deliveries, medications, exercise events, periods of stress, physiological events, manual insulin injections, and other health events,

entered via user inputs **34**. Bolus calculator module **48** uses the historical data to more accurately and efficiently determine the recommended insulin bolus and/or carbohydrate amount.

[0030] The bolus calculator module **48** determines a recommended bolus, such as an insulin correction bolus or a meal bolus, particular to the user based on the current glucose state, the history data, and user input. A suggested meal bolus (e.g., carbohydrate amount) may be in response to a detected or predicted hypoglycemic condition. A suggested correction bolus of insulin may be in response to the detected glucose exceeding the maximum allowable glucose level. The actual amount of carbohydrates consumed and the actual amount of insulin administered may be confirmed by the user as information entered via user inputs **34** and recorded in memory **39** with other history data. The recommended bolus may be displayed on display **28**.

[0031] Referring to FIG. 3, an exemplary CGM trace **100** is illustrated, wherein the x-axis represents time in minutes and the y-axis represents glucose in mg/dl. CGM trace **100** comprises a series of detected glucose levels measured over a period. In the illustrated embodiment, CGM trace **100** represents filtered glucose levels, i.e., glucose levels that are estimated based on the measured glucose levels weighted with the probably of sensor accuracy. A most recent estimated glucose level **110** has an associated negative rate of change indicated with arrow **112**. Bolus calculator module **48** determines the target glucose level **102** and a target range of glucose levels indicated with an upper glucose limit **104** and a lower glucose limit **106**. For illustrative purposes, target glucose level **102** is **110** mg/dl, upper glucose limit **104** is **140** mg/dl, and lower glucose limit **106** is **80** mg/dl, although other suitable values may be provided. Bolus calculator module **48** may determine target glucose level **102** and limits **104**, **106** based at least in part on the user's history data described herein. Management device **26** uses the trending glucose data of CGM trace **100** to recommend corrective action to move the blood glucose towards the target glucose level **102**. The target glucose level **102** of FIG. 3 corresponds to the maximum allowed glucose before time t_1 and after time t_2 , i.e., when there has not been any recent meals or correction boluses. Between times t_1 and t_2 , the maximum allowed glucose is adjusted based on a meal event **114** or other suitable events.

[0032] At time t_1 , meal event **114** occurs when the user consumes a meal and enters carbohydrate data into management device **26** indicating the amount of carbohydrates consumed with the meal. In some instances, an insulin bolus is administered at about the time of the meal event **114** to offset the expected increase in glucose levels resulting from the meal. Bolus calculator module **48** determines a projected glucose level rise and a duration of the glucose rise based on the carbohydrates consumed, the insulin correction bolus (if administered), and the user's historical data related to glucose swings following meals and insulin injections. Based on the projected glucose rise, bolus calculator module **48** determines an allowed rise value **124**, an offset time value **126**, and an acting time value **122**. The allowed rise value **124** may be based on other events, such as a glucagon injection, exercise, sleep,

driving, or time of day, for example.

[0033] The allowed rise value **124** is the amount by which the glucose level of the user may be allowed to increase with respect to the target glucose level **102** as a result of the carbohydrate intake and insulin bolus. In some embodiments, the allowed rise value **124** is the combination of a correction delta glucose value **130** resulting from an insulin bolus and a meal rise value **132** resulting from the meal event **114**. The correction delta glucose value **130** is the difference between the current glucose level and the target glucose level **102** at the time of the insulin bolus to allow time for the glucose level to decrease following insulin. As illustrated, the allowed rise value **124** is constant (see line **118**) for a first predetermined amount of time after the meal and insulin administration, i.e., offset time **126**, and then decreases linearly (see slope **120**) following the offset time **126**. The total time that the meal and insulin dose have an effect on the bG levels of a patient is the acting time **122**. FIG. 3 illustrates a trapezoid-shaped graph **116** of the allowed rise value **124** accounting for the effect of a dose of insulin and meal event.

[0034] The maximum allowed glucose increases based on allowed rise value **124** and follows plot **116** of FIG. 3. As such, bolus calculator module **48** expands the range of allowable glucose levels after a meal event for the duration of the acting time **122** according to plot **116**. The allowed rise value **124** illustratively has an initial height of 50 mg/dl, but could have other suitable heights based on the meal size, the insulin, and the user's typical reactions to boluses from the historical data. In some embodiments, for meal events above a threshold amount of carbohydrates, the meal rise value **132** is fixed. As one example, the offset time **126** is about two hours, and the acting time **122** is about three to five hours, depending on the user, the meal size, and the insulin bolus.

[0035] Referring again to FIG. 2, management device **26** further includes basal rate adjustment logic **50** operative to calculate and adjust a basal rate based on the current glucose state and the risk associated with the current glucose state. Management device **26** transmits an adjustment to the basal rate in a control signal to insulin pump **31** via communication link **35**, and insulin pump **31** adjusts the current insulin basal rate based on the adjustment. Alternatively, the adjusted basal rate may be displayed to the user, and the user manually adjusts the basal rate of insulin pump **31**. In one or more embodiment, the adjustment is a percent reduction to the initial, unadjusted or nominal basal rate based on a risk of hypoglycemia or a percent increase to the initial, unadjusted or nominal basal rate based on risk of hyperglycemic conditions.

[0036] The basal rate adjustment logic **50** determines whether the basal rate is to be adjusted. If an adjusted basal rate is proper, basal rate adjustment logic **50** calculates an adjusted basal rate and management device **26** transmits a control signal to insulin pump **31** to cause insulin pump **31** to deliver insulin at the adjusted basal rate. Alternatively, management device **26** may display the adjusted basal rate to the user to prompt the user for manual adjustment of the insulin pump **31**. In some embodiments, the implementation of the adjusted basal rate may be overridden by the user via manual control of the insulin pump **31**.

[0037] However, because control-to-range control of the continuous glucose monitoring system 10 must be able to work for a variety of people with diabetes and various lifestyles, the aggressiveness of the control-to-range control may be adjusted. Aggressiveness is the willingness of the CGM system 10 to increase the insulin delivered to the PWD 11. A more aggressive system is more likely to give more insulin to the PWD which results in more negative glucose velocities. The individual physiological characteristics and lifestyles of PWDs 11 may result in default settings for the control-to-range not being appropriate for every user of the continuous glucose monitoring system 10. Specifically, some PWD 11 may require a more hypoglycemic averse system or flexibility in their desired glucose range. Adjusting the aggressiveness of the control-to-range algorithm improves the safety of the continuous glucose monitoring system 10 by allowing the control-to-range to be customized to each PWD's 11 needs.

[0038] Additionally, the aggressiveness of the control-to-range may also be adjusted at different times of day or for different periods in the life cycle of the glucose sensor 16. For example, the aggressiveness may be reduced for the first day of use of a glucose sensor 16 and then subsequently increased when the glucose sensor 16 sensitivity has stabilized. The aggressiveness could also be reduced if no recent calibration blood glucose measurement has been taken. If no recent calibration blood glucose measurement has been taken, the accuracy of the CGM readings are less certain and the aggressiveness of the control-to-range is adjusted to account for the reduced confidence in the CGM reading accuracy.

[0039] As previously discussed, microcontroller 32 includes hazard analysis logic 40 that calculates target return paths from a plurality of initial glucose states to a target glucose state based on cumulative hazard values. FIG. 4C illustrates an exemplary hazard function 80 for calculating a hazard value for a given glucose level ultimately utilized in determination of the cumulative hazard value. In one or more embodiments the hazard function 80 is defined by the following equation:

$$h(g)_{hyper} = \max(\alpha_{hyper} \cdot \alpha (\log(\max(g - \Delta g_{hyper} - \max(\Delta g_{hypo}, 0), 1))^c - \beta), 0) \quad (1)$$

$$h(g)_{hypo} = \min(\alpha (\log(\max(g - \Delta g_{hypo}, 1))^c - \beta), 0) \quad (2)$$

$$h(g) = \begin{cases} h_{MAX} & \text{if } g - \Delta g_{hyper} - \max(\Delta g_{hypo}, 0) \geq g_{MAX} \\ h_{MIN} & \text{if } g - \Delta g_{hypo} \leq g_{MIN} \\ h(g)_{hyper} & \text{if } h(g)_{hypo} \geq 0 \\ h(g)_{hypo} & \text{if } h(g)_{hypo} < 0 \end{cases} \quad (3)$$

where g is the blood glucose value (mg/dl) shown on the x-axis, $h(g)$ is the corresponding hazard value shown on the y-axis, Δg_{hyper} is a hyperglycemic shift, Δg_{hypo} is a hypoglycemic shift, h_{MAX} is a maximum hazard, h_{MIN} is a minimum hazard, α_{hyper} is the hyperglycemic control aggressiveness, and α , β , and c are process variables. Additional and alternate hazard functions are also envisioned as outlined in the numerous related applications. In the illustrated embodiment, the variables α , β , and c are defined as follows: $\alpha = 1.509$, $\beta = 5.381$, and $c = 1.084$. g_{MAX} is a glucose value above which no additional incremental hazard is calculated

above h_{MAX} and similarly g_{MIN} is a glucose value below which no additional incremental hazard is calculated above h_{MIN} . Test cases of hazard functions for a hyperglycemic range ($h(g)_{hyper}$) and a hypoglycemic range ($h(g)_{hypo}$) are generated. The $h(g)$ function determines if h_{MAX} , h_{MIN} , $h(g)_{hyper}$, or $h(g)_{hypo}$ should be implemented as the final hazard value for the tested blood glucose value.

[0040] Implementation of g_{MAX} and g_{MIN} in the determination of h_{MAX} and h_{MIN} respectively prevent excessively positive or negative hazard values for extreme blood glucose values. In one or more embodiments g_{MAX} is set at 600 mg/dl and h_{MAX} is the $h(g)_{hyper}$ associated with g_{MAX} . Similarly, in one or more embodiments g_{MIN} is set at 10 mg/dl and h_{MIN} is the $h(g)_{hypo}$ associated with g_{MIN} . As such, if g exceeds g_{MAX} or drops below g_{MIN} , the hazard value associated with the blood glucose value is prevented from exceeding the range defined by h_{MAX} and h_{MIN} .

[0041] In one or more embodiments, the aggressiveness of the control-to-range is adjusted with a scaling of the risk surface. Specifically, a hyperglycemia risk scaling method introduces a scaling factor into the hazard function that only applies toward positive hazard values associated with hyperglycemia. Implementation of this hyperglycemia risk scaling method is achieved with the parameter α_{hyper} which provides functionality to adjust the aggressiveness of the hyperglycemic hazard function ($h(g)_{hyper}$) to account for the varying insulin sensitivities of PwD. Instituting a scaling factor results in a gradual reduction of the aggressiveness of the hyperglycemia portion of the risk surface and a concomitant gradual reduction of the aggressiveness of the adjustments to the basal rate. In scaling only the hyperglycemia hazard function, the hypoglycemia hazard evaluation is not affected. However, in further embodiments, a scaling factor could also be applied to the hypoglycemia risk surface so that the hypoglycemia risk and the hyperglycemia risk can be scaled independently.

[0042] With reference to FIGS. 4A and 4B, typical basal multipliers and basal multipliers with risk scaling are provided respectively. With typical basal multiplier, as illustrated in FIG. 4A, the basal rate would be increased to 250% at about 190 mg/dl and 0 mg/dl/min. Conversely, with hyperglycemic risk scaling, as illustrated in FIG. 4B, the basal rate would be decreased to about 165% at about 190 mg/dl and 0 mg/dl/min. The decreased aggressiveness is evidenced in the reduction of the basal multiplier from 250% to 165% with the risk scaling. Additionally, with reference to FIG. 4C, a nominal hazard function **80** is shown along with a hazard function with reduced α_{hyper} **82** illustrating the gradual reduction of the aggressiveness of the hazard function in the hyperglycemic region.

[0043] In one or more embodiments, the aggressiveness of the control-to-range is adjusted with shifting of the risk surfaces. Specifically, a hyperglycemia risk shifting method shifts the hyperglycemic risk surface to account for insulin on board following a meal or correction bolus. The hyperglycemia risk shift may also be used when a larger glucose target range is recommended for a patient. For example, children typically use a larger glucose target range.

In this case a minimum shift is used and any meal or bolus related shift is added. The hyperglycemic region of the risk surface is shifted by the meal rise or other shift in the maximum allowed glucose. In shifting only the hyperglycemia hazard function, the hypoglycemia hazard evaluation is not affected. Implementation of the hyperglycemic shift is illustrated in Equation 1 presented *supra* as the Δg_{hyper} parameter.

[0044] With reference to FIGS. 5A and 5B, typical basal multipliers and basal multipliers with risk shifting are provided respectively. With typical basal multipliers, as illustrated in FIG. 5A, the basal rate would be increased to 250% at about 190 mg/dl and 0 mg/dl/min. Conversely, with hyperglycemic risk shifting, as illustrated in FIG. 5B, the basal rate would remain substantially unchanged at about 100% at 190 mg/dl and 0 mg/dl/min. The decreased aggressiveness is evidenced in the reduction of the basal multiplier from 250% to 100% with the hypoglycemic risk shifting. With reference to FIG. 4C, Δg_{hyper} shifts the hazard function **80** in the hyperglycemic region (positive hazard values) to account for a recent meal or correction bolus. Hyper shift hazard function **84** illustrates a shift in the hazard function after a previous meal or correction bolus.

[0045] In one or more embodiments, the aggressiveness of the control-to-range is adjusted with modification of the allowed glucose acceleration. Glucose acceleration is the rate of change of glucose velocity. Glucose velocity is the rate of change of glucose value. As such glucose acceleration may have units of mg/dl/min² and glucose velocity may have units of mg/dl/min.

[0046] The risk surface calculation uses a parameter for the maximum allowed glucose acceleration when determining the hazard associated with a specific glucose state. Specifically, the cumulative hazard value of a return path from the current glucose state to the target glucose utilizes the maximum allowed glucose acceleration. A default value of glucose acceleration is 0.025 mg/dl/min² and adjusting the glucose acceleration value affects the shape of the risk surface. The maximum positive glucose acceleration and the maximum negative glucose acceleration may be different absolute values. If a person has glucagon available then their maximum positive acceleration may be increased while their maximum negative acceleration may remain unchanged. The availability of glucagon allows an overly aggressive insulin bolus or basal rate to be corrected.

[0047] The cumulative hazard value of a return path from the current glucose state to the target glucose state is calculated by summing the hazard values of the glucose values on the path between the current glucose state and the target glucose state. The path is constrained by limiting the maximum allowed glucose acceleration. Additionally, the target is assumed to have a rate-of-change of zero as once the target glucose state is reached it is desired to remain at the target glucose state and not oscillate above and below the target glucose state.

[0048] The return path of minimum risk between the glucose state and the target is the fastest path. This return path uses the maximum allowed glucose accelerations, both positive and

negative glucose accelerations, to return to the target glucose state. The closed form solution to the return path generation is composed of a time period with one extreme of the allowed glucose accelerations followed by the opposite extreme.

[0049] If a positive hypoglycemic shift is being used then the hypoglycemic shift must be added to the target glucose to get the shifted glucose target. This is necessary to correctly shift the hypoglycemic risk as the glucose target represents the blood glucose level where the hazard shifts from positive (hyperglycemic) to negative (hypoglycemic). The adjustment of the target glucose to the shifted glucose target is defined by the following equation:

$$\hat{g}_t = g_t + \max(\Delta g_{\text{hypo}}, 0) \quad (4)$$

where $\hat{g}_t$ is the shifted glucose target, g_t is the nominal glucose target, and Δg_{hypo} is the hypoglycemic shift. The maximum function in equation 4 prevents a negative hypoglycemic shift from being added to the target glucose and instead uses a hypoglycemic shift of zero resulting in $\hat{g}_t$ and g_t being equal.

[0050] As an initial matter, the generalized form of the return path must be determined. The return path may have an initial positive glucose acceleration followed by a negative glucose acceleration or may have an initial negative glucose acceleration followed by a positive glucose acceleration. The generalized form of the return path may be determined by solving which of equation 5 and equation 6, presented *infra*, returns a real number solution.

$$T^\pm = t_1^\pm + t_2^\pm \quad (5)$$

$$T^\mp = t_1^\mp + t_2^\mp \quad (6)$$

where

$$t_1^\pm = \frac{\sqrt{\ddot{g}_n(\ddot{g}_p - \ddot{g}_n)(-\dot{g}^2 + 2\ddot{g}_p - 2\hat{g}_t\ddot{g}_p) - \dot{g}\ddot{g}_p + \dot{g}\ddot{g}_n}}{\ddot{g}_p(\ddot{g}_p - \ddot{g}_n)}, \quad (7)$$

$$t_2^\pm = \frac{\dot{g} + \ddot{g}_p t_1^\pm}{-\ddot{g}_n}, \quad (8)$$

$$t_1^\mp = \frac{\sqrt{\ddot{g}_p(\ddot{g}_n - \ddot{g}_p)(-\dot{g}^2 + 2\ddot{g}_n - 2\hat{g}_t\ddot{g}_n) - \dot{g}\ddot{g}_n + \dot{g}\ddot{g}_p}}{\ddot{g}_n(\ddot{g}_n - \ddot{g}_p)}, \quad (9)$$

$$t_2^\mp = \frac{\dot{g} + \ddot{g}_n t_1^\mp}{-\ddot{g}_p}, \quad (10)$$

$\dot{g}$ is the rate of change of the glucose level, $\ddot{g}_p$ is the maximum positive glucose acceleration, $\ddot{g}_n$ is the maximum negative glucose acceleration, and $\hat{g}_t$ is the shifted glucose target from equation 4. If equation 5 returns a real number for $T^\pm$ and both

$$t_1^\pm$$

and

$$t_2^\pm$$

are greater than or equal to zero, the return path utilizes a positive acceleration first and a negative acceleration second. Conversely, if equation 6 returns a real number for $T^\mp$ and both

$$t_1^\mp$$

and

$t_2^{\mp}$

are greater than or equal to zero, the return path utilizes a negative acceleration first and a positive acceleration second.

[0051] Once the generalized form of the return path is determined, the cumulative hazard value of the return path may be calculated. When the return path utilizes a positive acceleration first, the cumulative hazard value is defined by the following equation:

$$h(g, \dot{g}) = \sum_{t=0}^{t_1^{\pm}} h\left(g + \dot{g}t + \frac{1}{2}\ddot{g}_p t^2\right) + \sum_{t=0}^{t_2^{\pm}} h\left(\hat{g}_t + \frac{1}{2}\ddot{g}_n t^2\right) \quad (11)$$

and when the return path utilizes a negative acceleration first, the cumulative hazard value is defined by the following equation:

$$h(g, \dot{g}) = \sum_{t=0}^{t_1^{\mp}} h\left(g + \dot{g}t + \frac{1}{2}\ddot{g}_n t^2\right) + \sum_{t=0}^{t_2^{\mp}} h\left(\hat{g}_t + \frac{1}{2}\ddot{g}_p t^2\right). \quad (12)$$

[0052] It should be appreciated that return paths that encounter more extreme glucose values will tend to have a higher cumulative hazard value as the hazard value for each time point is higher as illustrated in FIG. 4C. For example, a blood glucose value of 225 mg/dl would have a higher hazard value than a blood glucose value of 120 mg/dl at the same glucose rate-of-change. Also, paths that take a longer time to return to the target glucose state will tend to have a higher hazard value. A path may require longer returning to the target glucose state as a result of initial glucose rate-of-change or extreme glucose values.

[0053] In one or more embodiments, the allowed acceleration is increased. Increasing the allowed acceleration results in a reduced risk for larger rates of change in glucose concentration because the CGM system 10 assumes that it is easier to recover from an undesirable glucose state with the higher allowed maximum acceleration. Adjusting the control-to-range system with an increased maximum allowed acceleration causes the control-to-range system to wait longer to reduce the basal insulin rate when blood glucose is falling which thereby increases the aggressiveness. With reference to FIGS. 6A and 6B, the basal rate when the rate of change in the glucose concentration (glucose velocity) is zero are almost identical between the default settings and the control-to-range system with the increased aggressiveness from an increased maximum allowed acceleration implemented. The resulting negative slope of the basal multiplier with respect to the rate of change of the glucose concentration is reduced.

[0054] In one or more embodiments, the allowed acceleration is decreased. Decreasing the allowed acceleration results in the CGM system 10 calculating a greater risk for increased rates of change in the glucose concentration. The increased calculated risk in rate of change of the blood glucose concentration deviating from zero makes the CGM system 10 react quickly to any drop or rise in glucose. The CGM system 10 aggressively manages any deviation from a zero rate of change in glucose concentration. With reference to FIGS. 7A and 7B, the basal rate when the rate of change in the glucose concentration (glucose velocity) is zero are almost identical between the default settings and the control-to-range system with the increased

aggressiveness from an increased maximum allowed acceleration implemented. The resulting negative slope of the basal multiplier with respect to the rate of change of the glucose concentration is increased.

[0055] In one or more embodiments, the risk is determined by summing the hazard of a range of glucose states multiplied by the probability of that state. The glucose state uncertainty controls the calculation of the probability of a given state. As previously discussed, the uncertainty is typically produced by the Kalman filter. If the uncertainty remains high for an extended period of time or crosses a specific threshold then the PWD **11** is notified and the control algorithm may be changed from control-to-range to predictive low glucose suspend (pLGS). If the uncertainty crosses a more extreme threshold, the control system may be turned off until the glucose sensor **16** of the CGM system **10** is recalibrated or replaced.

[0056] The cumulative hazard value provides the hazard for a specific return path from the current glucose state to the target glucose state. However, there are uncertainties in CGM blood glucose measurements from glucose sensor **16**. As such, the true blood glucose measurement may vary from the blood glucose determined by the glucose sensor **16** and the specific calculated cumulative hazard value may be inaccurate with regards to the actual return path. To account for the variability in the true return path, a current risk metric is determined which accounts for variance in the CGM blood glucose measurements.

[0057] To calculate the current risk metric, a predicted glucose state at an intermediate point of the CTR period is initially determined. In various embodiments, the intermediate point of the CTR period is the true midpoint (1/2 of the CTR period), 1/4 of the CTR period, 1/3 of the CTR period, 2/3 the CTR period, or 3/4 of the CTR period. In an embodiment, the CTR is typically updated every 15 minutes resulting in the midpoint being 7.5 minutes into the 15 minute sampling interval. For short time horizons a linear prediction performs as well or better than more complicated models, so a linear prediction is used for simplicity. The rate-of-change in the glucose level is assumed to remain constant over the 7.5 min window in determining the predicted blood glucose level at the midpoint of the 15 minute sampling interval. As such, the predicted glucose level is defined by the following equation:

$$\hat{g} = g + \dot{g}\tau \quad (13)$$

where g is the initial measured blood glucose level, $\dot{g}$ is the initial rate-of-change of the glucose level, and τ is the prediction time measured from the beginning of the CTR period. The predicted glucose state is thus $[\hat{g}, \dot{g}]$.

[0058] Subsequently, a glucose state distribution around the predicted glucose state is determined. Similarly, a glucose state distribution around the current glucose state may also be determined. The samples for the glucose state distribution are selected based on the standard deviation of the distribution in the g and $\dot{g}$ directions. Generation of the glucose state distribution samples is defined by the following equations:

$$G_s = \left[g - 2\sigma_g, g - 2\sigma_g + \frac{4\sigma_g}{k}, g - 2\sigma_g + 2\frac{4\sigma_g}{k}, g - 2\sigma_g + 3\frac{4\sigma_g}{k}, \dots, g - 2\sigma_g + k\frac{4\sigma_g}{k} \right] \quad (14)$$

$$G_s = \left[g - 2\sigma_g, g - 2\sigma_g + \frac{4\sigma_g}{k}, g - 2\sigma_g + 2\frac{4\sigma_g}{k}, g - 2\sigma_g + 3\frac{4\sigma_g}{k}, \dots, g - 2\sigma_g + k\frac{4\sigma_g}{k} \right]$$

$$\hat{G}_s = \left[\dot{g} - 2\sigma_{\dot{g}}, \dot{g} - 2\sigma_{\dot{g}} + \frac{\sim g}{n}, \dot{g} - 2\sigma_{\dot{g}} + 2\frac{\sim g}{n}, \dot{g} - 2\sigma_{\dot{g}} + 3\frac{\sim g}{n}, \dots, \dot{g} - 2\sigma_{\dot{g}} + n\frac{\sim g}{n} \right] \quad (15)$$

where G_s is the distribution of glucose values, $\hat{G}_s$ is the distribution of glucose rates of change, g is the glucose value for the current risk metric, $\dot{g}$ is the rate of change of the glucose level for the current risk metric, σ_g is the standard deviation of g , $\sigma_{\dot{g}}$ is the standard deviation of $\dot{g}$, k is the number of divisions of G_s , and n is the number of divisions of $\hat{G}_s$. It will be appreciated that g may represent the current glucose level or the predicted glucose level if the glucose state distribution is desired for the current glucose state or the predicted glucose state respectively. Equation 14 and equation 15 provide a distribution of samples ranging within two standard deviations of g and $\dot{g}$. In at least one embodiment, the sampled values for g are selected by dividing the range bounded by two standard deviations by 10 and the sampled values for $\dot{g}$ are selected by dividing the range bounded by two standard deviations by 8 such that $k = 10$ and $n = 8$ respectively.

[0059] The current risk metric is determined based on a weighted average of the cumulative hazard values of the return paths generated from each of the sampled glucose states. Specifically, the risk is calculated by determining the weighted average of the cumulative hazard values at each combination of points in G_s and $\hat{G}_s$ and weighting them by a multivariate exponential function $w(g_s, \dot{g}_s)$. The current risk metric is defined by the following equation:

$$r = \frac{\sum_{G_s} \sum_{\hat{G}_s} h(g_s, \dot{g}_s) w(g_s, \dot{g}_s)}{\sum_{G_s} \sum_{\hat{G}_s} w(g_s, \dot{g}_s)} \quad (16)$$

where r is the current risk metric,

$$w(g_s, \dot{g}_s) = \exp\left(-\frac{1}{2} \begin{bmatrix} g_s - g & \dot{g}_s - \dot{g} \end{bmatrix} P_g^{-1} \begin{bmatrix} g_s - g \\ \dot{g}_s - \dot{g} \end{bmatrix}\right), \quad (17)$$

G_s is the distribution of glucose values and $\hat{G}_s$ is the distribution of glucose rates of change determined from the glucose state distribution around the detected glucose state, $h(g_s, \dot{g}_s)$ is the cumulative hazard value of the return path at each glucose state, g is the glucose value for the current risk metric, $\dot{g}$ is the rate of change of the glucose level for the current risk metric,

$$P_g = \begin{bmatrix} \sigma_g^2 & \sigma_g \sigma_{\dot{g}} \\ \sigma_g \sigma_{\dot{g}} & \sigma_{\dot{g}}^2 \end{bmatrix}, \quad (18)$$

σ_g is the standard deviation of g , and $\sigma_{\dot{g}}$ is the standard deviation of $\dot{g}$. The weighting of the cumulative hazard values results in samples closest to the measured glucose state receiving the largest weight in the final current risk metric calculation.

[0060] In one or more embodiments, the uncertainty in the glucose state is increased. Increasing the uncertainty causes an increase in the probability of hypoglycemia. Additionally, since the hazard function is asymmetric, the increased probability of hypoglycemia leads to an increase in the risk of hypoglycemia. The increase in the risk of hypoglycemia results in the control-to-range system reacting sooner to increases in rates of change of blood glucose (glucose velocity) and also decreases the aggressiveness of a basal increase in the hyperglycemic region. With reference to FIGS. 8A and 8B, the basal multiplier of a typical uncertainty and an increased uncertainty are provided respectively. With a typical uncertainty, as illustrated in FIG. 8A, the basal rate would be increased to 250% at about 190 mg/dl and 0

mg/dl/min. Conversely, with an increased uncertainty, as illustrated in FIG. 8B, the basal rate would be increased to about 210% at about 190 mg/dl and 0 mg/dl/min. The decreased aggressiveness is evidenced in the reduction of the basal multiplier from 250% to 210% with an increase in the uncertainty of the glucose state.

[0061] In further embodiments, the uncertainty in the glucose state is decreased. Decreasing the uncertainty causes the control-to-range system to increase its trust in the glucose state. The increase in the trust in the glucose state results in the control-to-range system reacting more slowly to increases in rates of change of blood glucose (glucose velocity) and also increases the aggressiveness of a basal increase in the hyperglycemic region. The control-to-range system may react more slowly to increases in rates of change of blood glucose because the probability of actually being in hypoglycemia is reduced with the decreased uncertainty in the glucose state. With reference to FIGS. 9A and 9B, the basal multiplier of a typical uncertainty and a decreased uncertainty are provided respectively. The region where no adjustment to the basal rate is requested is increased with a decreased uncertainty in the glucose state as shown in a comparison of FIGS. 9A and 9B.

[0062] Each of the aggressiveness parameters may be adjusted by the PWD 11 manually or by the control-to-range algorithm based on other factors such as exercise, stress, sleep, travel, age, and/or illness.

[0063] The glucose uncertainty and/or acceleration parameters may be used in an algorithm to determine the risk surface and/or basal multiplier profile, but not exposed to the PWD 11 or user. For example, the PWD 11 or user may be given the choice of low, medium, or high aggressiveness which adjusts maximum allowed glucose acceleration, hyperglycemic risk shifting, hypoglycemic risk shifting, and risk scaling to achieve the desired result. The abstract setting of low, medium, or high aggressiveness may be achieved without alerting the PWD 11 or HCP to the particular values utilized for the 4 aggressiveness parameters. It will be appreciated that additional levels of aggressiveness may also be implemented such as medium-low and medium-high or a scale of 1-10 representing 10 distinct aggressiveness strata.

[0064] In further embodiments, the HCP and PWD 11 may define a specific range which is set using the hyperglycemic shift parameter and an aggressiveness which is set using the scaling factor and acceleration.

[0065] The parameters which determine aggressiveness of the CGM system 10 may be set when the CGM system 10 is first prescribed and then optimized over time. In some embodiments the aggressiveness setting could be medium as the default setting with adjustment to a more aggressive high setting or a less aggressive low setting.

[0066] In adjusting and/or determining the aggressiveness setting, the HCP and/or PWD 11 may look to the sensitivity of the PWD 11 to both negative and positive glucose velocities. Some people are distressed as much by a rapid negative glucose velocity when their blood

glucose is still at a good range as they are by going hypoglycemic. Additionally, the HCP could utilize a questionnaire to gauge the PWD's 11 fear of hypoglycemia, the PWD's 11 degree of knowledge regarding times of hypoglycemia, and the number of recent severe hypoglycemic episodes as a guide for selecting the aggressiveness setting of low, medium, or high.

[0067] The final basal multiplier for each CTR period is determined utilizing the current risk metric. The current risk metric is first converted to a basal multiplier value between 0 and TBR_{MAX} . TBR_{MAX} is the maximum percentage for a temporary basal rate (TBR). In at least one embodiment, the TBR_{MAX} defaults to 250%. In further embodiments, the TBR_{MAX} is lower or higher than 250% and is adjusted to tune the control and determination for hypo-adverse individuals. The basal multiplier value is defined by the following equation:

$$BM(r) = \begin{cases} \frac{r-r_{0\%}}{-r_{0\%}}, & r > r_{0\%} \\ 0, & r \leq r_{0\%} \end{cases} \quad (19)$$

where $BM(r)$ is the basal multiplier value, r is the current risk metric, and $r_{0\%}$ is a reference risk metric. In one or more embodiments, the reference risk metric is a glucose state linked to complete basal shutoff. For example, complete basal shutoff may occur at 70 mg/dl such that when the blood glucose level is below 70 mg/dl no basal insulin is provided. The basal multiplier value may be provided as a continuous function as the current risk metric varies. However, before providing the adjusted basal rate to the therapy delivery device **31** it is converted to the nearest TBR increment (TBR_{inc}) to provide an incremental basal rate multiplier (BM_{inc}). The incremental basal rate multiplier is defined by the following equation:

$$BM_{inc} = \min\left(\max\left(\text{floor}\left(\frac{BM(r)}{TBR_{inc}}\right)TBR_{inc}, 0\right), TBR_{MAX}\right). \quad (20)$$

With reference to FIG. 9, exemplary continuous basal multiplier values and incremental basal rate multipliers with a TBR_{inc} of 10% and the implemented floor function are illustrated.

[0068] It is to be appreciated that a barrier to adoption of an automatic control strategy for insulin delivery systems has been the uncertainty in the input data, i.e. the glucose values, from a continuous glucose sensor(s). Great effort has been made in improving the accuracy and reliability. For example, even with impedance data being used to adjust the data from the glucose sensor to improve the accuracy of the reported value, a reliability of 100% is probably not likely to be achieved. For this reason, a gain control module may evaluate the quality of the sensor data, and accounts for the quality in the control algorithm. Specifically, the inventors have discovered that a probability score derived from the time course of sensor data and used to adapt the gain of a statistical filter can improve the quality of the reported value. The Sensor Quality Score Q_{total} can also be used to adapt the controller gain of the insulin delivery system, such that the aggressiveness of the control can be traded off against the safety of the user based on the degree of confidence in the sensor glucose results.

[0069] The aggressiveness of the controller can be adjusted using the Sensor Quality Score. In the case of proportional-integral-derivative controller (PID) control, the controller is specified with three gain terms.

$$u(t) = K_p e(t) + K_i \int_0^t e(\tau) d\tau + K_d \frac{de(t)}{dt} \quad (21)$$

The Sensor Quality Score may be used to adjust some set of the gain terms.

$$K_p = Q_{total} k_p \quad (22)$$

$$K_i = Q_{total} k_i \quad (23)$$

$$K_d = Q_{total} k_d \quad (24)$$

Additionally the Sensor Quality Score can be used when calculating the integral term so that past errors that occur when the sensor quality is low have less impact on the current controller output.

$$u(t) = K_p e(t) + K_i \int_0^t Q_{total}(\tau) e(\tau) d\tau + K_d \frac{de(t)}{dt} \quad (25)$$

[0070] The aggressiveness of the controller may also be adjusted using a hyper shift, hyper scaling, max allowed glucose acceleration, or glucose state uncertainty. The hyper shift may be zero when Q_{total} is one and increase as it decreases toward zero. The hyper scaling may be equal to Q_{total} or a factor of it. The glucose state uncertainty is adjusted by incorporating the Q_{total} value into the recursive filter.

[0071] The quality of data being evaluated is assessed in terms of a total quality score Q_{total} from a set of quality metrics, e.g., of signal input characteristic(s) and data received from the glucose sensor 16 and/or an impedance sensor. The total quality score Q_{total} has a value that ranges from zero (0) to (one) 1, and is used to alter the gain of the microcontroller 32 to provide an increased level of safety when the quality score is low, and to improve microcontroller performance and glycemic control when the quality score is high.

[0072] For example, in one illustrated implementation, in the case of a sensor 16 with a total quality score, $Q_{total} = 0$ (or $0 \leq Q_{total} < T$), the microcontroller 32 if operating in closed-loop glucose control, in which insulin delivery adjustments are made automatically by the microcontroller 32 based on the received input from the glucose sensor 16, would fall back to a safer, open-loop mode of operation, i.e., open-loop glucose control, in which adjustments are made by the user and as recommended to the user by pre-programmed time profiles. In the case of the total quality score Q_{total} being greater than a threshold value T and/or equal to one (1), i.e., $T < Q_{total} \leq 1$, the microcontroller 32 acts more aggressively to manage glycemia with the certainty that the sensor data will enable the system to deliver the proper amount of insulin, thereby allowing, e.g., the system 10 to function in optimal closed-loop glucose control with optimal safety.

[0073] In another implementation, in the case of the total quality score Q_{total} being greater than a threshold value T_{high} and/or equal to one (1), i.e., $T_{high} < Q_{total} \leq 1$, the microcontroller 32 acts aggressively to manage glycemia with the certainty that the sensor data will enable the system to deliver the proper amount of insulin, thereby allowing, e.g., the system 10 to function in optimal closed-loop glucose control with optimal safety. In the case of a glucose sensor 16 with a total quality score, Q_{total} such that $T_{low} \leq Q_{total} < T_{high}$, where $T_{low} < T_{high}$ the

microcontroller 32 would fall back to a safer, reduced-gain closed-loop mode of operation, in which adjustments are made automatically by the microcontroller, but with a reduced gain based on the value of the total quality score through implementation of equations 21-25. In the case of a sensor 16 with a total quality score, Q_{total} such that $0 \leq Q_{total} < T_{low}$, the microcontroller would fall back to a safer, open-loop mode of operation, i.e., open-loop glucose control, in which adjustments are made by the user and as recommended to the user by pre-programmed time profiles and as recommended to the user by pre-programmed time profiles

[0074] For further and alternative descriptions for probability based controller gain and Q_{total} see U.S. patent application Ser. No. 15/061,202, filed on March 4, 2016, entitled "Probability Based Controller Gain". For further and alternative descriptions for determining the basal rate adjustment, see U.S. patent application Ser. No. 14/229,016, filed on March 28, 2015, entitled "System and Method for Adjusting Therapy Based on Risk Associated with a Glucose State". For further description of calculating the target return paths and calculating risk metrics, see U.S. patent application Ser. No. 13/645,198, filed on Oct. 4, 2012, entitled "System and Method for Assessing Risk Associated with a Glucose State". For further description of the probability analysis tool, the recursive filter, the uncertainty calculation, and other probability and risk analysis functionalities of computing device 66, see U.S. patent application Ser. No. 12/693,701, filed on Jan. 26, 2010, entitled "Methods and Systems for Processing Glucose Data Measured from a Person Having Diabetes," and U.S. patent application Ser. No. 12/818,795, filed on Jun. 18, 2010, entitled "Insulin Optimization Systems and Testing Methods with Adjusted Exit Criterion Accounting for System Noise Associated with Biomarkers". For further description of the bolus calculator module 88, see U.S. patent application Ser. No. 13/593,557, filed on Aug. 24, 2012, entitled "Handheld Diabetes Management Device with Bolus Calculator," and U.S. patent application Ser. No. 13/593,575, filed on Aug. 24, 2012, entitled "Insulin Pump and Methods for Operating the Insulin Pump".

[0075] It should now be understood that the methods and systems described herein may be used to estimate the glucose level of a person having diabetes and utilize a control-to-range algorithm to adjust the glucose level of a person having diabetes. Furthermore, the methods and systems described herein may also be used to tune the aggressiveness of the control-to-range algorithm to reliably increase insulin basal rates to account for increases in glucose concentration. The methods described herein may be stored on a computer-readable medium which has computer-executable instructions for performing the methods. Such computer-readable media may include compact discs, hard drives, thumb drives, random-access memory, dynamic random-access memory, flash memory, and so forth.

[0076] It is noted that recitations herein of a component of the present disclosure being "configured" in a particular way, "configured" to embody a particular property, or function in a particular manner, are structural recitations, as opposed to recitations of intended use. More specifically, the references herein to the manner in which a component is "configured" denotes an existing physical condition of the component and, as such, is to be taken as a definite recitation of the structural characteristics of the component.

REFERENCES CITED IN THE DESCRIPTION

Cited references

This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.

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- [US17045016 \[0001\]](#)
- [US2015273147A1 \[0004\]](#)
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- KOVATCHEV, B. P. et al.Symmetrization of the blood glucose measurement scale and its applicationsDiabetes Care, 1997, vol. 20, 1655-1658 [\[0007\]](#)

PATENTKRAV

1. Fremgangsmåde til bestemmelse af en basalhastighedsjustering af insulin i et kontinuerligt glukoseovervågningssystem (10) hos en person med diabetes (11), hvilken fremgangsmåde omfatter:

- ved hjælp af mindst én computeranordning at modtage et signal, der er repræsentativt for mindst én glukosemåling;

- ved hjælp af den mindst ene computeranordning at påvise en glukosetilstand for personen baseret på signalet, hvilken påvist glukosetilstand indbefatter et glukoseniveau (110) for personen og en ændringshastighed af glukoseniveauet (112);

- ved hjælp af den mindst ene computeranordning at bestemme en aktuel risikometrik, hvilken aktuel risikometrik angiver en risiko for mindst én af en hypoglykæmisk tilstand og en hyperglykæmisk tilstand hos personen, hvor bestemmelsen af den aktuelle risikometrik omfatter

- ved hjælp af den mindst ene computeranordning at bestemme en tilbagevej baseret på en overgang fra den påviste glukosetilstand til en målglukosetilstand, hvilken tilbagevej omfatter mindst én mellemliggende glukoseværdi, der er forbundet med en tilbagevenden til målglukosetilstanden;

- ved hjælp af den mindst ene computeranordning at bestemme fareværdier for et givet glukoseniveau (110) af den mindst ene mellemliggende glukoseværdi med en farefunktion (80), idet hver fareværdi indikerer en fare forbundet med den tilsvarende mellemliggende glukoseværdi;

- ved hjælp af den mindst ene computeranordning at bestemme en kumulativ fareværdi for tilbagevejen, hvilken kumulativ fareværdi indbefatter en sum af fareværdierne for den mindst ene glukoseværdi på tilbagevejen; og

- ved hjælp af den mindst ene computeranordning at bestemme et vægtet gennemsnit af kumulative fareværdier for tilbageveje, der er genereret fra en glukosetilstandsfordeling omkring den påviste glukosetilstand; og

- ved hjælp af den mindst ene computeranordning at beregne en justering til en basalhastighed af en behandlingsleveringsanordning baseret på den aktuelle risikometrik og en kontrol-til-område-algoritme, der omfatter mindst én aggressivitetsparameter, hvilken aggressivitetsparameter er valgt blandt:

(a) at tilvejebringe en skaleringsparameter α_{hyper} , der er omfattet af farefunktionen (80), for at justere positive fareværdier forbundet med hyperglykæmi

(82);

(b) at tilvejebringe en forskydningsparameter Δg_{hyper} , der er omfattet af farefunktionen (80), for at forskyde positive fareværdier (84) for at tage højde for insulinindhold efter et måltid (114) eller en korrektionsbolus;

5 (c) at justere til en maksimalt tilladt glukoseacceleration, der anvendes af tilbagevejen, idet glukoseacceleration repræsenterer hastigheden af ændring af glukosehastighed, og glukosehastighed (112) repræsenterer hastigheden af ændring af glukoseværdier;

10 (d) at justere til en glukosetilstandsusikkerhed, der repræsenterer niveauet af tillid til den målte glukosetilstand, for at vægte glukosetilstandene; eller

(e) kombinationer deraf;

hvor fareværdien for hver af fareværdierne for den mindst ene glukoseværdi på tilbagevejen bestemmes af den mindst ene computeranordning i overensstemmelse med en farefunktion (80) som følger

$$15 \quad h(g)_{hyper} = \text{maks.} (\alpha_{hyper} \cdot \alpha (\log(\text{maks.} (g - \Delta g_{hyper} - \text{maks.} (\Delta g_{hypo}, 0)), 1))^c - \beta), 0),$$

$$h(g)_{hypo} = \text{min.} (\alpha (\log(\text{maks.} (g - \Delta g_{hypo}, 1))^c - \beta), 0), \text{ og}$$

$$h(g) = \begin{cases} h_{MAKS.} & \text{hvis } g - \Delta g_{hyper} - \text{maks.} (\Delta g_{hypo}, 0) \geq g_{MAKS.} \\ h_{MIN.} & \text{hvis } g - \Delta g_{hypo} \leq g_{MIN.} \\ h(g)_{hyper} & \text{hvis } h(g)_{hypo} \geq 0 \\ h(g)_{hypo} & \text{hvis } h(g)_{hypo} < 0 \end{cases}$$

20 hvor g er glukoseværdien, Δg_{hyper} er en hyperglykæmisk forskydning for at tage højde for et nyligt måltid (114) eller en korrektionsbolus, Δg_{hypo} er en hyperglykæmisk forskydning for at tage højde for nylig træning eller glucagon, $h_{MAKS.}$ er en maksimal fareværdi, der repræsenterer faren for en glukoseværdi på 600 mg/dl, $g_{MAKS.}$ er en glukoseværdi, over hvilken der ikke beregnes yderligere trinvis fare over $h_{MAKS.}$, $h_{MIN.}$ er en minimumsfare, der repræsenterer fareværdien for en glukoseværdi på 10 mg/dl, $g_{MIN.}$ er en glukoseværdi, under hvilken der ikke beregnes yderligere trinvis fare over $h_{MIN.}$, α_{hyper} er den hyperglykæmiske kontrolaggressivitet for at justere for insulinfølsomhed, og α , β og c er beregningsvariabler.

2. Fremgangsmåde ifølge krav 1, der yderligere omfatter visning af grafiske data, der repræsenterer den beregnede justering af basalhastigheden, til en bruger på en grafisk brugergrænseflade.

3. Fremgangsmåde ifølge krav 1, der yderligere omfatter generering af et basalt multiplikatorplot baseret på den aktuelle risikometrik.

4. Fremgangsmåde ifølge krav 1, hvor

- hvis $T^\pm = t_1^\pm + t_2^\pm$ er et reelt tal, bestemmes den kumulative fareværdi for tilbagevejen af den mindst ene computeranordning i overensstemmelse med

$$h(g, \dot{g}) = \sum_{t=0}^{t_1^\pm} h\left(g + \dot{g}t + \frac{1}{2}\ddot{g}_p t^2\right) + \sum_{t=0}^{t_2^\pm} h\left(\hat{g}_t + \frac{1}{2}\ddot{g}_n t^2\right)$$

5 hvor

$$t_1^\pm = \frac{\sqrt{\ddot{g}_n(\ddot{g}_p - \ddot{g}_n)(-\dot{g}^2 + 2\ddot{g}_p - 2\ddot{g}_t\ddot{g}_p) - \dot{g}\ddot{g}_p + \ddot{g}_n}}{\ddot{g}_p(\ddot{g}_p - \ddot{g}_n)}, \quad t_2^\pm = \frac{\dot{g} + \ddot{g}_p t_1^\pm}{-\ddot{g}_n},$$

$\dot{g}$ er ændringshastigheden af glukoseniveauet (112), $\ddot{g}_p$ er den maksimale positive glukoseacceleration, og $\ddot{g}_n$ er den maksimale negative glukoseacceleration, eller

- hvis $T^\mp = t_1^\mp + t_2^\mp$ er et reelt tal, bestemmes den kumulative fareværdi for tilbagevejen af

10 den mindst ene computeranordning i overensstemmelse med

$$h(g, \dot{g}) = \sum_{t=0}^{t_1^\mp} h\left(g + \dot{g}t + \frac{1}{2}\ddot{g}_n t^2\right) + \sum_{t=0}^{t_2^\mp} h\left(\hat{g}_t + \frac{1}{2}\ddot{g}_p t^2\right)$$

hvor

$$t_1^\mp = \frac{\sqrt{\ddot{g}_p(\ddot{g}_n - \ddot{g}_p)(-\dot{g}^2 + 2\ddot{g}_n - 2\ddot{g}_t\ddot{g}_n) - \dot{g}\ddot{g}_n + \ddot{g}_p}}{\ddot{g}_n(\ddot{g}_n - \ddot{g}_p)}, \quad t_2^\mp = \frac{\dot{g} + \ddot{g}_n t_1^\mp}{\ddot{g}_p},$$

$\dot{g}$ er ændringshastigheden af glukoseniveauet (112), $\ddot{g}_p$ er den maksimale positive glukoseacceleration, og $\ddot{g}_n$ er den

15 maksimale negative glukoseacceleration.

5. Fremgangsmåde ifølge krav 1, hvor kun risikooverfladen, der repræsenterer hyperglykæmisk risiko, forskydes.

6. Fremgangsmåde ifølge krav 5, hvor forskydningen i den hyperglykæmiske risikooverflade korrigerer for insulinindhold efter et måltid (114) eller en korrektionsbolus.

20 7. Fremgangsmåde ifølge krav 1, hvor den maksimalt tilladte glukoseacceleration øges.

8. Fremgangsmåde ifølge krav 1, hvor den maksimalt tilladte glukoseacceleration sænkes.

9. Fremgangsmåde ifølge krav 1, hvor glukosetilstandsusikkerheden frembringes af et Kalman-filter.

25 10. Fremgangsmåde ifølge krav 1, hvor glukosetilstandsfordelingen bestemmes af den mindst ene computeranordning i overensstemmelse med

$$G_s = \left[g - 2\sigma_g, g - 2\sigma_g + \frac{4\sigma_g}{k}, g - 2\sigma_g + 2\frac{4\sigma_g}{k}, g - 2\sigma_g + 3\frac{4\sigma_g}{k}, \dots, g - 2\sigma_g + k\frac{4\sigma_g}{k} \right] \text{ og}$$

$$\dot{G}_s = \left[\dot{g} - 2\sigma_{\dot{g}}, \dot{g} - 2\sigma_{\dot{g}} + \frac{4\sigma_{\dot{g}}}{n}, \dot{g} - 2\sigma_{\dot{g}} + 2\frac{4\sigma_{\dot{g}}}{n}, \dot{g} - 2\sigma_{\dot{g}} + 3\frac{4\sigma_{\dot{g}}}{n}, \dots, \dot{g} - 2\sigma_{\dot{g}} + n\frac{4\sigma_{\dot{g}}}{n} \right]$$

hvor G_s er fordelingen af glukoseværdier, $\dot{G}_s$ er fordelingen af glukoseændringshastigheder, g er glukoseværdien for den aktuelle risikomåling, $\dot{g}$ er ændringshastigheden af glukoseniveauet (112) for den aktuelle risikomåling, σ_g er standardafvigelsen for g , $\sigma_{\dot{g}}$ er standardafvigelsen for $\dot{g}$, k er antallet af divisioner af G_s , og n er antallet af divisioner af $\dot{G}_s$.

11. Fremgangsmåde ifølge krav 1, hvor den aktuelle risikometrik bestemmes af den mindst ene computeranordning i overensstemmelse med

$$r = \frac{\sum_{G_s} \sum_{\dot{G}_s} h(g_s, \dot{g}_s) w(g_s, \dot{g}_s)}{\sum_{G_s} \sum_{\dot{G}_s} w(g_s, \dot{g}_s)}$$

10 hvor r er den aktuelle risikomåling, $w(g_s, \dot{g}_s) = \exp. = \left(-\frac{1}{2} [g_s - g \quad \dot{g}_s - \dot{g}] P_g^{-1} \begin{bmatrix} g_s - g \\ \dot{g}_s - \dot{g} \end{bmatrix} \right)$, G_s er fordelingen af glukoseværdier, og $\dot{G}_s$ er fordelingen af glukoseændringshastigheder bestemt ud fra glukosetilstandsfordelingen omkring den påviste glukosetilstand, $h(g_s, \dot{g}_s)$ er den kumulative fareværdi for tilbagevejen ved hver glukosetilstand, g er glukoseværdien for den aktuelle risikomåling, $\dot{g}$ er ændringshastigheden af glukoseniveauet (112) for den aktuelle risikomåling, $P_g = \begin{bmatrix} \sigma_g^2 & \sigma_g \sigma_{\dot{g}} \\ \sigma_g \sigma_{\dot{g}} & \sigma_{\dot{g}}^2 \end{bmatrix}$, σ_g er standardafvigelsen for g , og $\sigma_{\dot{g}}$ er standardafvigelsen for $\dot{g}$.

12. Blodglukosestyringsanordning (26), der er konfigureret til at bestemme en basalhastighedjustering i et kontinuerligt glukoseovervågningssystem for en person med diabetes (11), hvilken anordning omfatter:

- 20 - et uforgængeligt computerlæsbart medium, der lagrer udførlige instruktioner; og
- mindst én behandlingsanordning, der er konfigureret til at udføre de udførlige instruktioner, således at de udførlige instruktioner, når de udføres af den mindst ene behandlingsanordning, får den mindst ene behandlingsanordning til at:
 - modtage et signal, der repræsenterer mindst én glukosemåling;
 - 25 - at påvise en glukosetilstand for personen baseret på signalet, hvilken påvist glukosetilstand indbefatter et glukoseniveau (110) for personen og en ændringshastighed af glukoseniveauet (112);
 - at bestemme en aktuel risikometrik, hvilken aktuel risikometrik angiver en risiko for mindst én af en hypoglykæmisk tilstand og en hyperglykæmisk tilstand hos
 - 30 en person, hvor bestemmelsen af den aktuelle risikometrik omfatter

- ved hjælp af den mindst ene computeranordning at bestemme en tilbagevej baseret på en overgang fra den påviste glukosetilstand til en målglukosetilstand, hvilken tilbagevej omfatter mindst én mellemliggende glukoseværdi, der er forbundet med en tilbagevenden til målglukosetilstanden;

5 - ved hjælp af den mindst ene computeranordning at bestemme fareværdier for et givet glukoseniveau (110) af den mindst ene mellemliggende glukoseværdi med en farefunktion (80), idet hver fareværdi indikerer en fare forbundet med den tilsvarende mellemliggende glukoseværdi;

10 - ved hjælp af den mindst ene computeranordning at bestemme en kumulativ fareværdi for tilbagevejen, hvilken kumulativ fareværdi indbefatter en sum af fareværdierne for den mindst ene glukoseværdi på tilbagevejen; og

- ved hjælp af den mindst ene computeranordning at bestemme et vægtet gennemsnit af kumulative fareværdier for tilbageveje, der er genereret fra en glukosetilstandsfordeling omkring den påviste glukosetilstand; og

15 - at beregne en justering til en basalhastighed af en behandlingslevering baseret på den aktuelle risikometrik og en kontrol-til-område-algoritme, der omfatter mindst én aggressivitetsparameter, hvilken aggressivitetsparameter er valgt blandt:

20 (a) at tilvejebringe en skaleringsparameter α_{hyper} , der er omfattet af farefunktionen (80), for at justere positive fareværdier forbundet med hyperglykæmi (82);

(b) at tilvejebringe en forskydningsparameter Δg_{hyper} , der er omfattet af farefunktionen (80), for at forskyde positive fareværdier (84) for at tage højde for insulinindhold efter et måltid (114) eller en korrektionsbolus;

25 (c) at justere til en maksimalt tilladt glukoseacceleration, der anvendes af tilbagevejen, idet glukoseacceleration repræsenterer hastigheden af ændring af glukosehastighed, og glukosehastighed repræsenterer hastigheden af ændring af glukoseværdier (112);

30 (d) at justere til en glukosetilstandsusikkerhed, der repræsenterer niveauet af tillid til den målte glukosetilstand, for at vægte glukosetilstandene; eller

(e) kombinationer deraf;

hvor fareværdien for hver af fareværdierne for den mindst ene glukoseværdi på tilbagevejen bestemmes af den mindst ene computeranordning i overensstemmelse med en

farefunktion (80) som følger

$$h(g)_{hyper} = \text{maks.} (\alpha_{hyper} \cdot \alpha(\log(\text{maks.} (g - \Delta g_{hyper} - \text{maks.} (\Delta g_{hypo}, 0), 1))^c - \beta), 0),$$

$$h(g)_{hypo} = \text{min.} (\alpha(\log(\text{maks.} (g - \Delta g_{hypo}, 1))^c - \beta), 0), \text{ og}$$

$$h(g) = \begin{cases} h_{MAKS.} & \text{hvis } g - \Delta g_{hyper} - \text{maks.} (\Delta g_{hypo}, 0) \geq g_{MAKS.} \\ h_{MIN.} & \text{hvis } g - \Delta g_{hypo} \leq g_{MIN.} \\ h(g)_{hyper} & \text{hvis } h(g)_{hypo} \geq 0 \\ h(g)_{hypo} & \text{hvis } h(g)_{hypo} < 0 \end{cases}$$

- 5 hvor g er glukoseværdien, Δg_{hyper} er en hyperglykæmisk forskydning for at tage højde for et nyligt måltid (114) eller en korrektionsbolus, Δg_{hypo} er en hyperglykæmisk forskydning for at tage højde for nylig træning eller glucagon, $h_{MAKS.}$ er en maksimal fareværdi, der repræsenterer faren for en glukoseværdi på 600 mg/dl, $g_{MAKS.}$ er en glukoseværdi, over hvilken der ikke beregnes yderligere trinvis fare over $h_{MAKS.}$, $h_{MIN.}$ er en minimumsfare, der
- 10 repræsenterer fareværdien for en glukoseværdi på 10 mg/dl, $g_{MIN.}$ er en glukoseværdi, under hvilken der ikke beregnes yderligere trinvis fare over $h_{MIN.}$, α_{hyper} er den hyperglykæmiske kontrolaggressivitet for at justere for insulinfølsomhed, og α , β og c er beregningsvariabler.

DRAWINGS

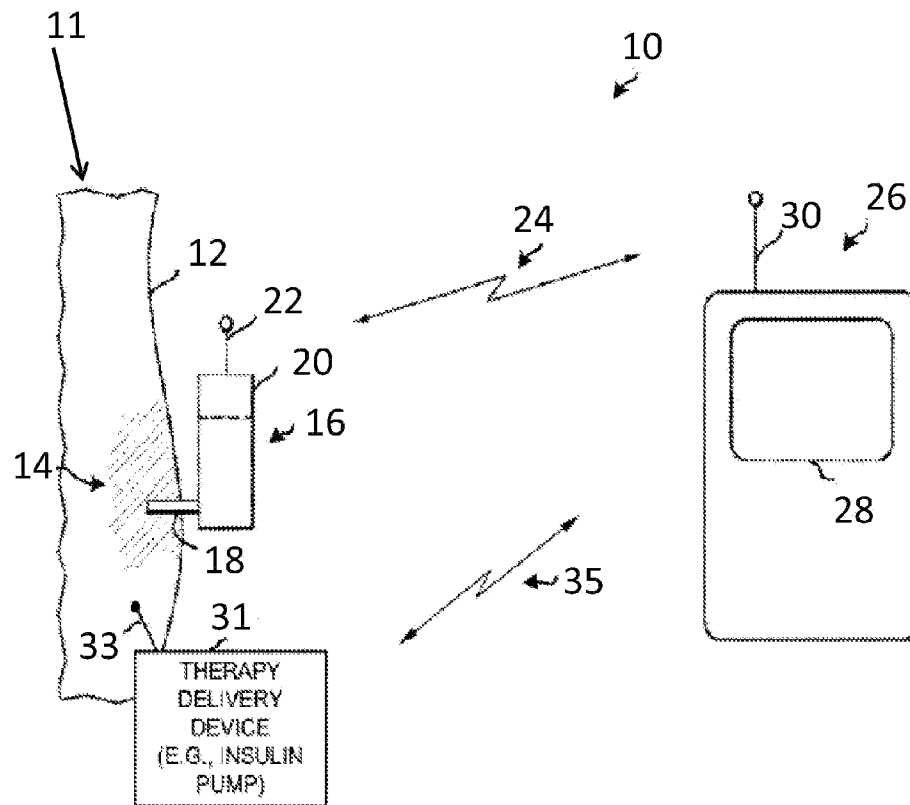


FIG. 1

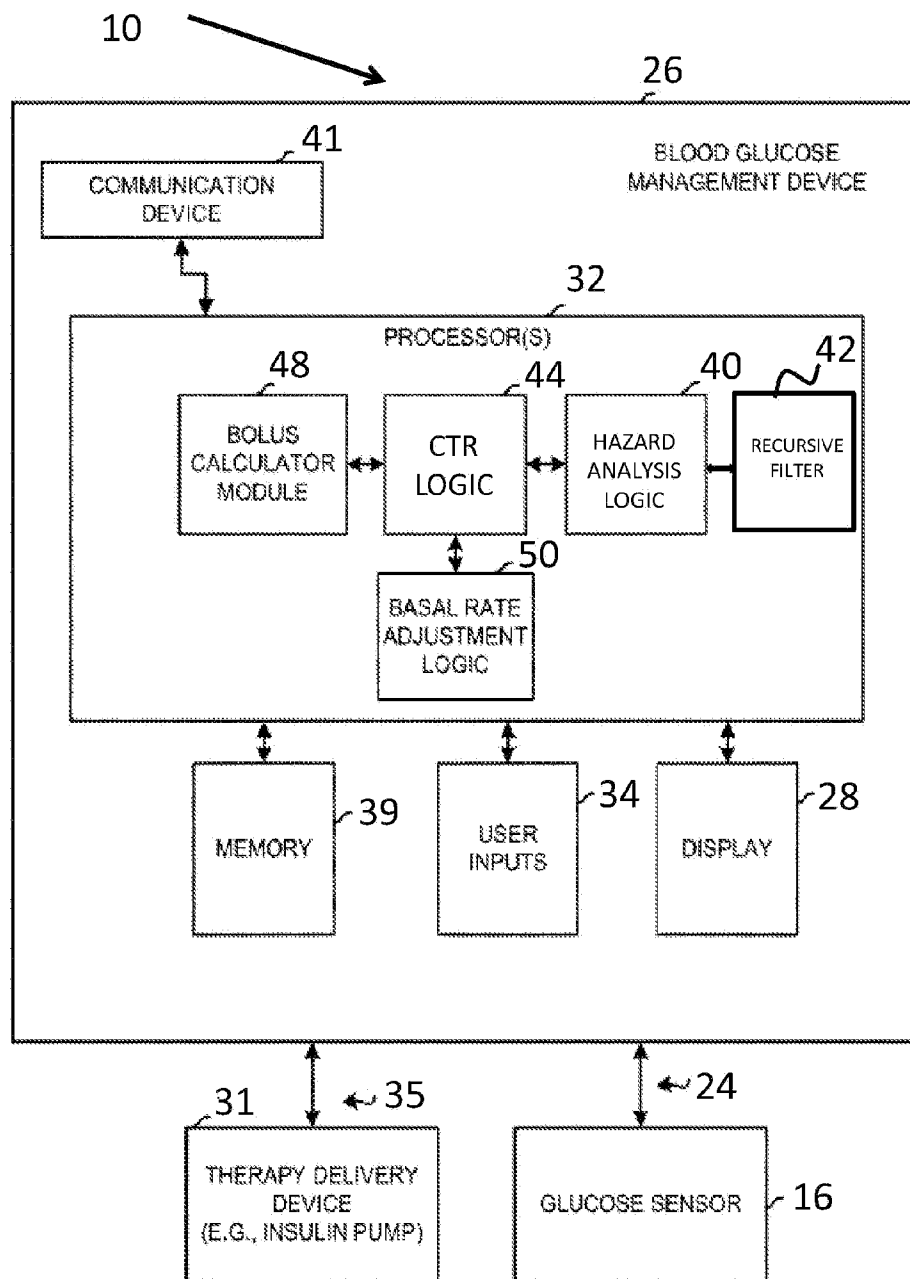


FIG. 2

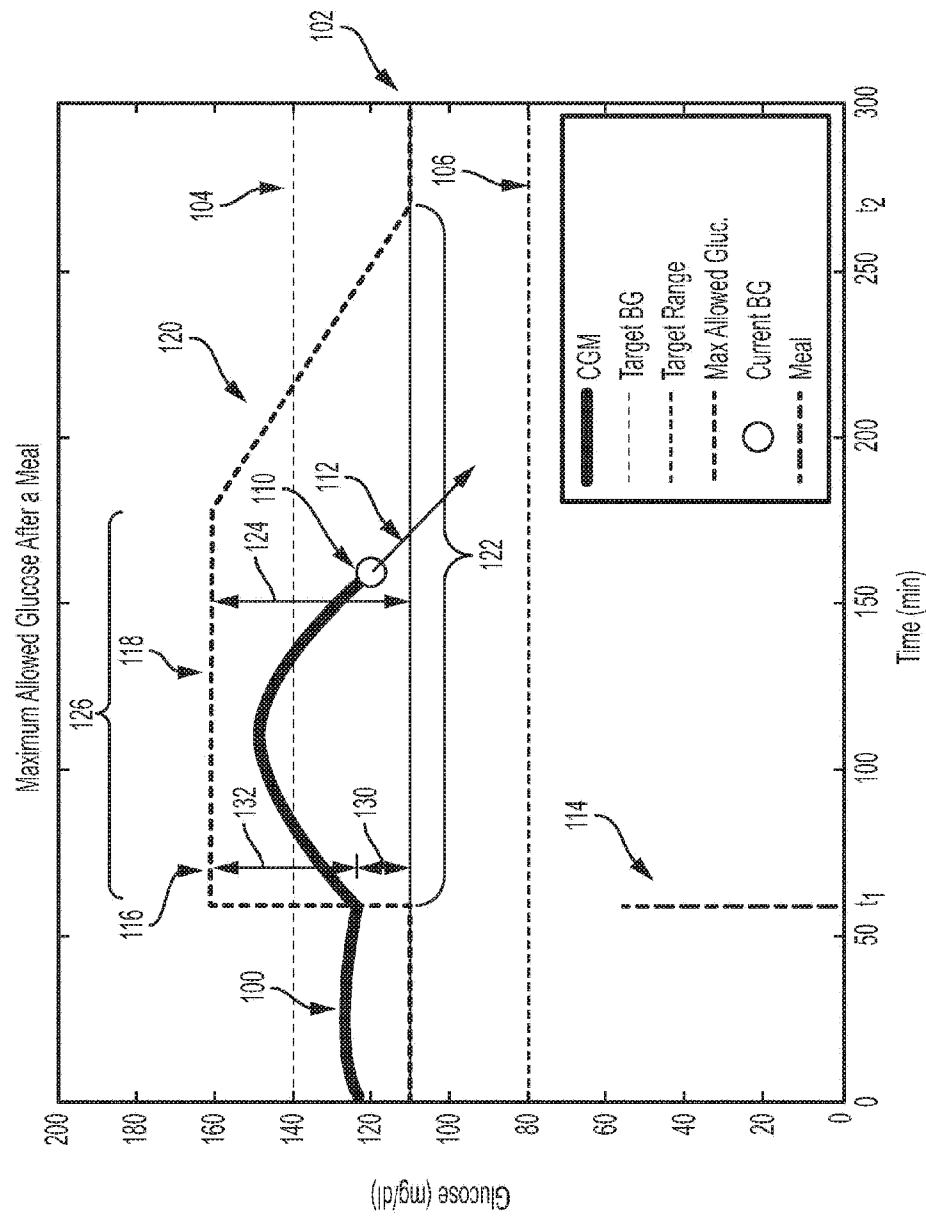


FIG. 3

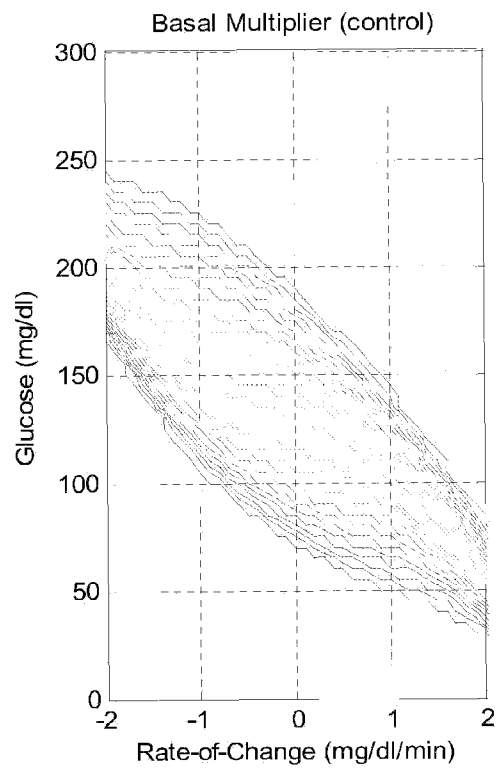


FIG. 4A

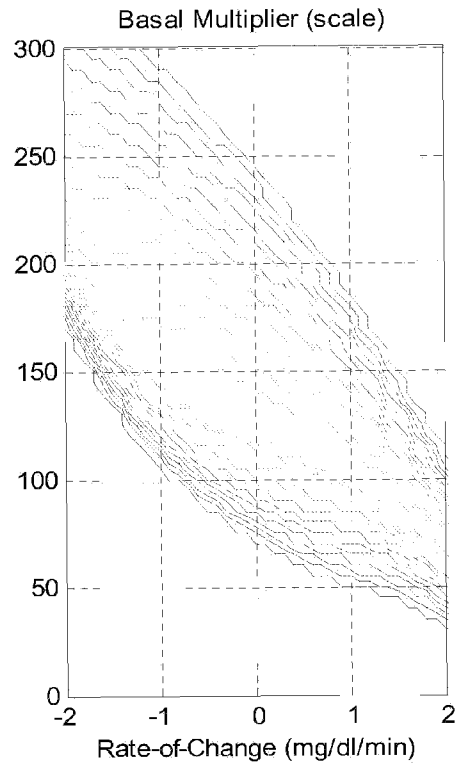


FIG. 4B

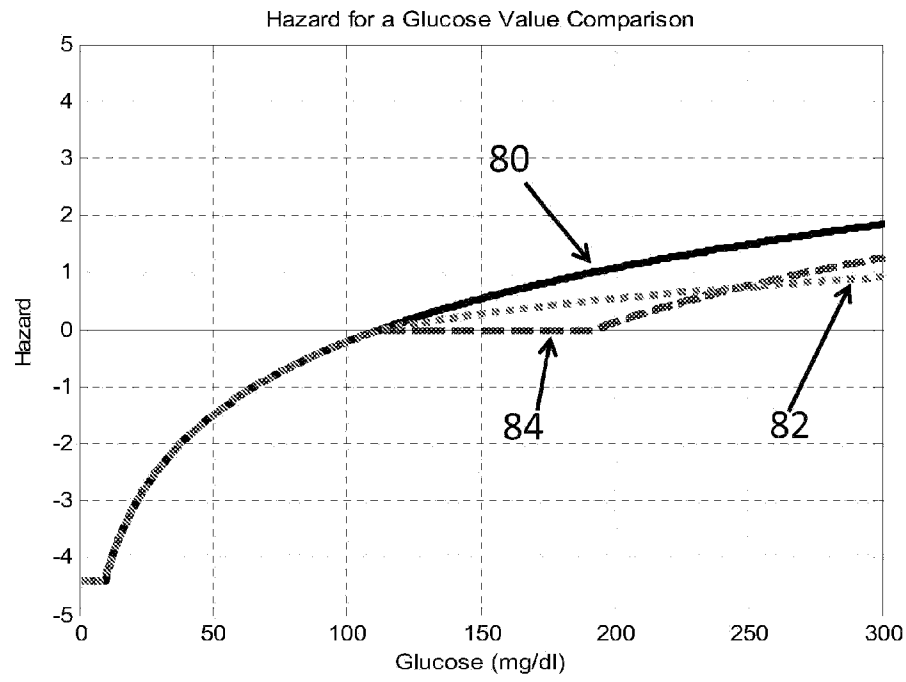


FIG. 4C

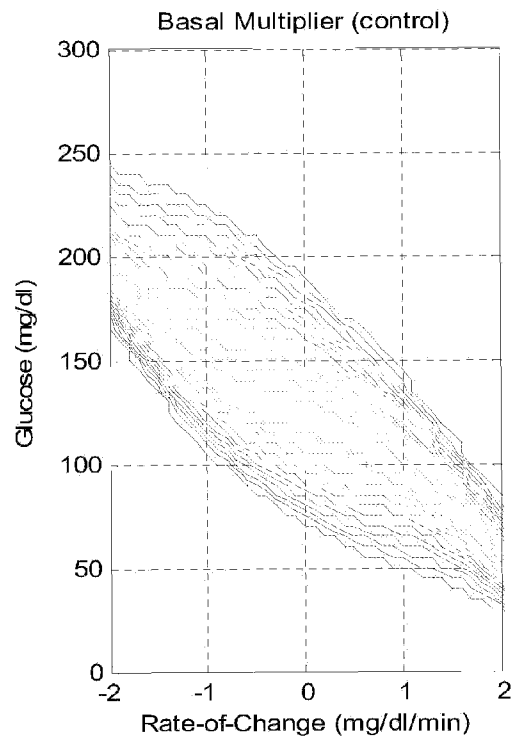


FIG. 5A

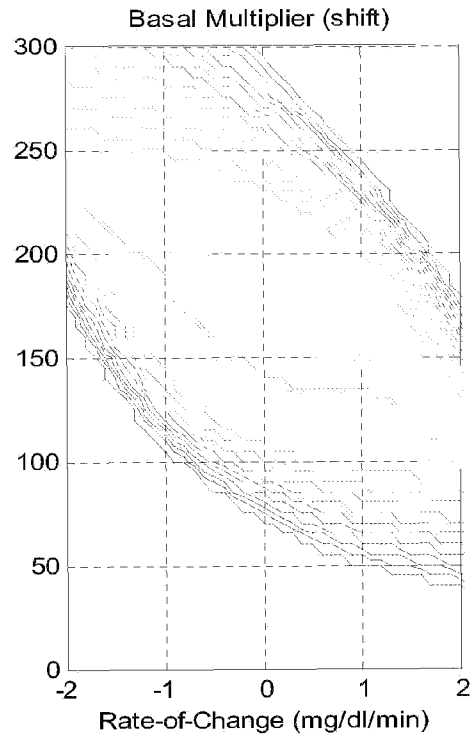


FIG. 5B

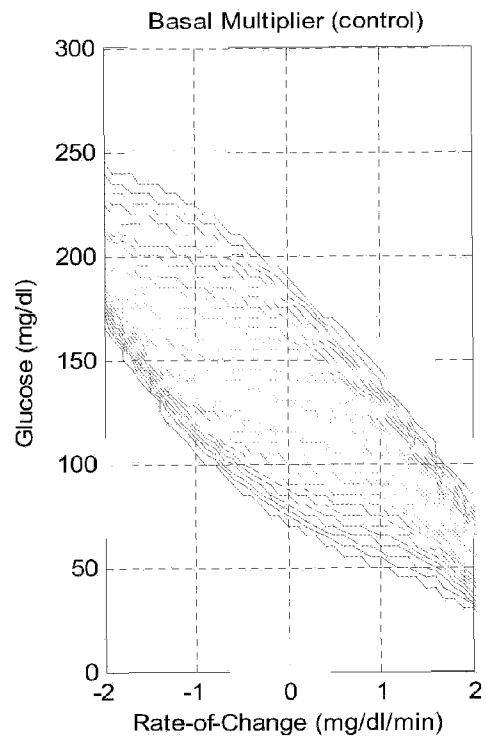


FIG. 6A

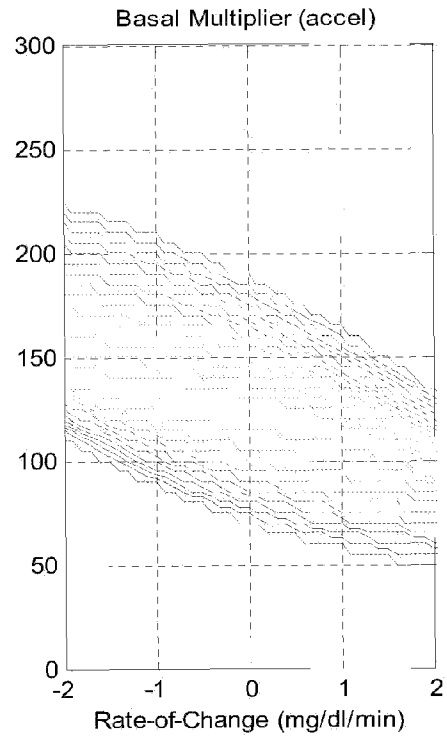


FIG. 6B

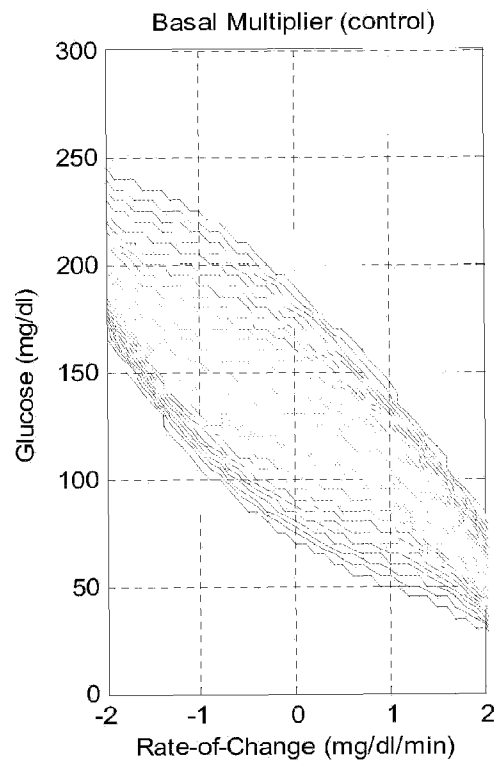


FIG. 7A

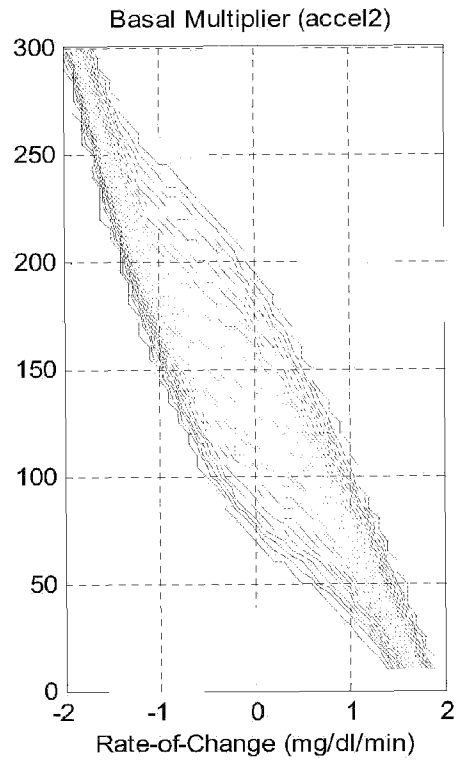


FIG. 7B

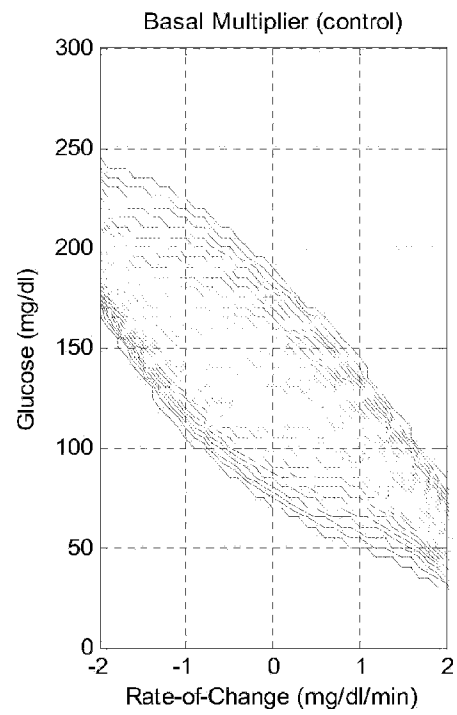


FIG. 8A

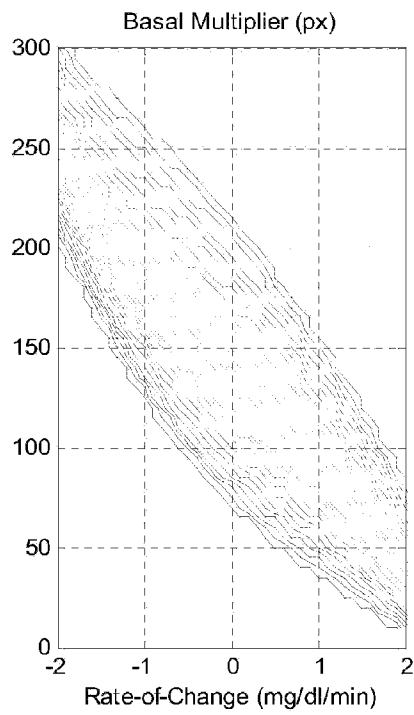


FIG. 8B

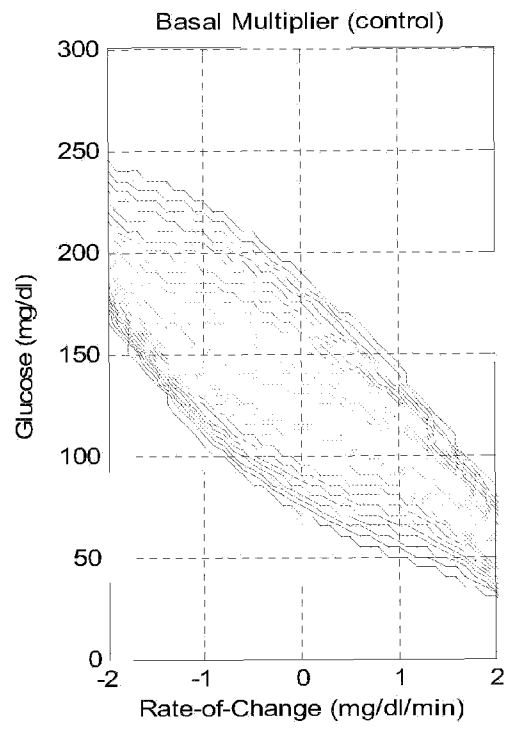


FIG. 9A

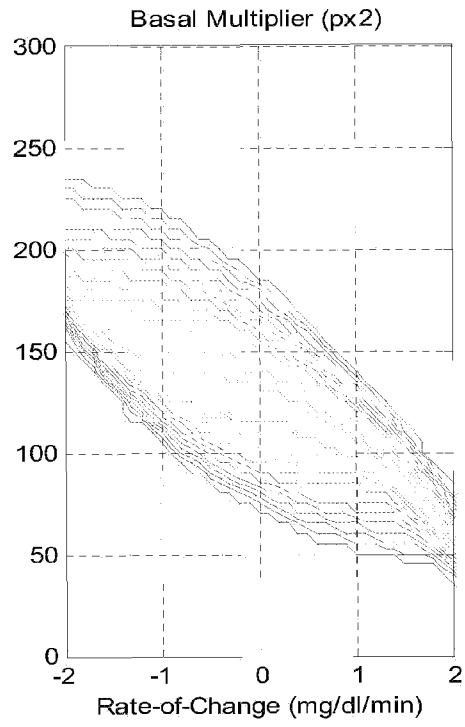


FIG. 9B