



(22) Date de dépôt/Filing Date: 2011/03/22
(41) Mise à la disp. pub./Open to Public Insp.: 2011/10/29
(30) Priorité/Priority: 2010/04/29 (US12/770,508)

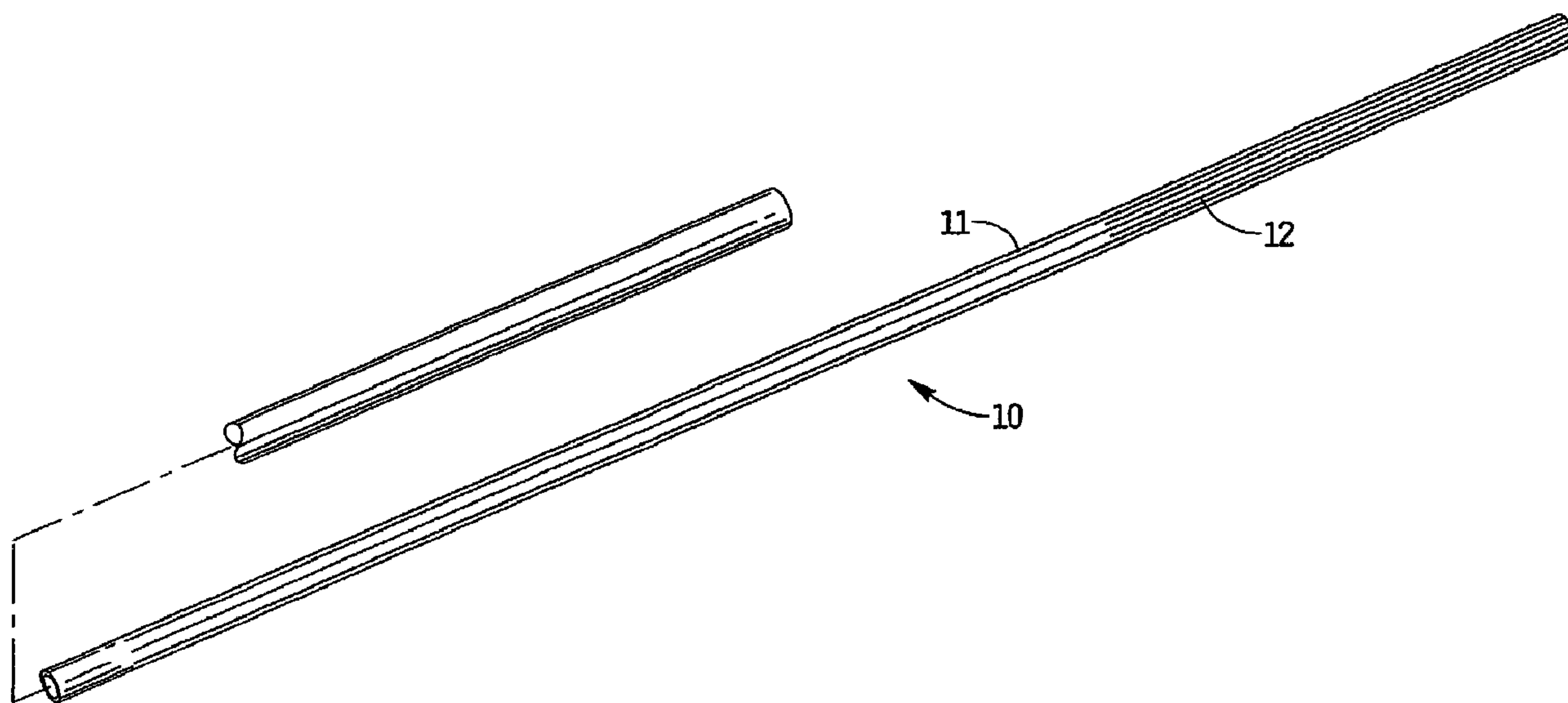
(51) Cl.Int./Int.Cl. *A61F 2/01* (2006.01)

(71) Demandeur/Applicant:
REX MEDICAL, L.P., US

(72) Inventeurs/Inventors:
MCGUCKIN, JAMES, F., JR., US;
BRESSLER, JAMES, E., US;
THINNES, JOHN H., JR., US;
DEFONZO, STEPHAN A., US;
CARTER, LINDSAY L., US

(74) Agent: MCFADDEN, FINCHAM

(54) Titre : **FILTRE VEINEUX**
(54) Title: **VEIN FILTER**



(57) **Abrégé/Abstract:**

A vessel filter having a first region and a second region, the filter movable between a collapsed position for delivery to the vessel and an expanded position for placement within the vessel. The first region has a filter portion having a converging region to direct particles toward the center of the filter and includes a plurality of spaced apart filter struts. The struts each have a strut height defined as a distance between a first wall and a second wall. A plurality of hooks are at the second region, the hooks having a vessel penetrating tip and a width greater than the width of the strut from which it extends such that the penetrating tip portion of the hook extends beyond the first wall.

ABSTRACT

A vessel filter having a first region and a second region, the filter movable
5 between a collapsed position for delivery to the vessel and an expanded position for
placement within the vessel. The first region has a filter portion having a converging
region to direct particles toward the center of the filter and includes a plurality of spaced
apart filter struts. The struts each have a strut height defined as a distance between a first
wall and a second wall. A plurality of hooks are at the second region, the hooks having a
10 vessel penetrating tip and a width greater than the width of the strut from which it extends
such that the penetrating tip portion of the hook extends beyond the first wall.

VEIN FILTER

BACKGROUND

5

Technical Field

This application relates to a vascular filter and more particularly to a vein filter for capturing blood clots within the vessel.

10 Background of Related Art

Passage of blood clots to the lungs is known as pulmonary embolism. These clots typically originate in the veins of the lower limbs and can migrate through the vascular system to the lungs where they can obstruct blood flow and therefore interfere with oxygenation of the blood. Pulmonary embolisms can also cause shock and even death.

15 In some instances, blood thinning medication, e.g. anticoagulants such as Heparin, or sodium warfarin can be given to the patient. These medications, however, have limited use since they may not be able to be administered to patients after surgery or stroke or given to patients with high risk of internal bleeding. Also, this medication approach is not always effective in preventing recurring blood clots.

20 Therefore, surgical methods to reduce the likelihood of such pulmonary embolisms by actually blocking the blood clot from reaching the lungs have been developed. One surgical method of treatment involved major surgery where the size of the vessel lumen was restricted by placement of ligatures or clips around the vein, e.g. the inferior vena cava which transports blood from the lower portion of the body to the heart
25 and lungs. This prevented passage of dangerously large blood clots through the vein to the lungs. However, this approach is an invasive surgical procedure, requiring an abdominal incision and general anesthesia and frequently causing vessel thrombosis and lower extremity swelling. Also, there is a lengthy patient recovery time and additional hospital and surgeon expenses associated with this major surgery. In fact, oftentimes, the
30 patients requiring the surgery are unhealthy and the major surgery and general anesthesia poses a risk in and of itself.

To avoid such invasive surgery, less invasive surgical techniques have been developed. These involve the placement of a mechanical barrier in the inferior vena cava. These barriers are in the form of filters and are typically inserted through either the femoral vein in the patient's leg or the right jugular vein in the patient's neck or arm
5 under local anesthesia. The filters are then advanced intravascularly to the inferior vena cava where they are expanded to block migration of the blood clots from the lower portion of the body to the heart and lungs.

These prior filters take various forms. One type of filter is composed of coiled wires such as disclosed in U.S. Patent nos. 5,893,869 and 6,059,825. Another type of
10 filter consists of legs with free ends having anchors for embedding in the vessel wall to hold the filter. These filters are disclosed, for example, in U.S. Patent nos. 4,688,553, 4,781,173, 4,832,055, and 5,059,205, 5,984,947 and 6,007,558. Another type of filter is disclosed in U.S. Patent no. 6,214,025 consisting of wires twisted together to form a cylindrical anchoring portion conforming to the inner vessel wall surface to exert a radial
15 force and a conical filtering portion.

Several factors have to be considered in designing vein filters. One factor is that the filter needs to be securely anchored within the vessel wall, while avoiding traumatic engagement and damage to the wall as well as damage to the neighboring abdominal aorta. Another factor is that the filter must be collapsible to a sufficiently small size to be
20 easily maneuvered and atraumatically advanced intravascularly to the inferior vena cava or other target vessel. Thirdly, the filter should direct the blood clots to the center of the vessel to improve dissolution of the clot within the vessel by the blood flow.

It would be advantageous to provide a vein filter that satisfies the foregoing parameters. Namely, such vein filter would advantageously have sufficient anchoring
25 force to retain the filter within the vessel while providing atraumatic contact with the vessel wall, would have a minimized insertion (collapsed) profile to facilitate delivery through the vascular system to the surgical site, and would enable migration of the captured blood clots to the center of the vessel. Moreover, it would also be advantageous to provide a filter that could simplify insertion through the femoral or the right jugular
30 vein or arm into the inferior vena cava.

Additionally, the need for a vein filter in many patients is temporary. In these instances it would be advantageous to provide a vein filter that satisfies the foregoing factors and in addition could be readily removed from the patient. Thus, the filter would advantageously strike the balance of having structure to provide sufficient anchoring while enabling atraumatic removal from the vessel after a period of time. It would further be advantageous if the filter could be removed minimally invasively, e.g. intravascularly.

SUMMARY

The present invention provides in one aspect a vessel filter comprising a first region and a second region, the filter movable between a collapsed position for delivery to the vessel and an expanded position for placement within the vessel. The first region has a filter portion having a converging region to direct particles toward the center of the filter and includes a plurality of spaced apart filter struts. The struts each have a strut width defined as a distance between a first wall and a second wall. A plurality of hooks are at the second region, each of the hooks having a vessel penetrating tip, positioned on a distal end portion of the strut, and having a width greater than the width of the strut from which it extends such that the penetrating tip portion of the hook extends radially beyond the first wall.

In one embodiment, the hooks have a curved end surface. Preferably, the hook includes a heel extending at an angle to a longitudinal axis of the strut. In a preferred embodiment, the penetrating tip extends in a direction toward the first region and the heel extends in an opposite direction.

The filter is preferably formed from a laser cut tube and composed of shape memory material. Preferably the filter includes a retrieval hook having a cutout exposing an internal annular surface, the annular surface dimensioned to receive a portion of a retrieval sheath.

In some embodiments, connecting filter struts extend at an angle from the filter struts to join adjacent filter struts.

In a preferred embodiment, the hooks include a plurality of teeth extending in an opposite direction of the penetrating tip. Preferably, the heel extends radially beyond the second wall of the respective strut.

In another aspect of the present invention, the vessel filter comprises a body made from a single tube, the tube cut to create a plurality of elongated struts forming a filter region and a mounting region of greater transverse dimension. The mounting region includes a plurality of vessel engaging hooks, each of the hooks having a penetrating tip
5 pointing in a direction toward the filter region, a plurality of teeth for engaging the vessel, and a heel extending beyond the teeth in a direction opposite the direction of the penetrating tip.

In one embodiment, the penetrating tip extends substantially parallel to the longitudinal axis of the strut.

10 In a preferred embodiment, the heel of the hook extends at an angle to the longitudinal axis of the struts in the mounting region. In one embodiment, the heel of adjacent vessel engaging hooks terminate axially spaced. In one embodiment, the heel of one hook is longitudinally aligned with the penetrating tip of an adjacent hook.

The present invention provides in another aspect a vessel filter comprising a first
15 region and a second region, the filter movable between a collapsed position for delivery to the vessel and an expanded position for placement within the vessel. The first region has a filter portion having a converging region to direct particles toward the center of the filter, the first region including a plurality of spaced apart filter struts, the struts each having a strut width defined as a distance between a first wall and a second wall. A
20 plurality of hooks are provided at the second region, each hook having a vessel penetrating tip and a heel, the penetrating tip of one hook longitudinally aligned with a portion of the heel of an adjacent hook.

In one embodiment, the hook has a third and fourth wall and a second width defined between the third and fourth walls, the second width greater than the width of the
25 strut from which it extends such that the penetrating tip portion of the hook extends radially beyond the first wall. In one embodiment, the heel of the hook extends beyond the second wall of the strut. The strut can have a reduced diameter area transitioning into the hook, the reduced area providing a space to accommodate a heel of an adjacent hook. In one embodiment, the penetrating tip of the hook points toward the first region. In one
30 embodiment, the heel has a width less than the width of the respective strut. The hook can have a heel that extends at an angle to the longitudinal axis.

BRIEF DESCRIPTION OF THE DRAWINGS

Preferred embodiment(s) of the present disclosure are described herein with reference to the drawings wherein:

5 Figure 1 is a perspective view of a first embodiment of the vein filter of the present invention in the collapsed configuration;

 Figure 2 is an enlarged side view of a portion of the vein filter of Figure 1;

 Figure 3 is a perspective view of the vein filter of Figure 1 in an expanded configuration;

10 Figure 4A is a side view of the vein filter of Figure 1 in another expanded configuration;

 Figure 4B is a front view of the vein filter of Figure 4 in the expanded configuration;

 Figure 5 is a side view of the vein filter of Figure 3 in the expanded configuration;

15 Figure 6A is a close up view of a portion of the struts showing one embodiment of anchoring elements having pointed ends;

 Figure 6B is a close up view of a portion of one of the struts showing another embodiment of anchoring elements in the form of hemispherical cutouts;

20 Figure 7 is a perspective view of an alternate embodiment of the vein filter of the present invention shown in the expanded configuration;

 Figure 8 is a side view of the vein filter of Figure 7;

 Figure 9 is a side view of a portion of the vein filter of Figure 7 shown in the collapsed configuration;

25 Figure 10 is a perspective view of another alternate embodiment of the vein filter of the present invention shown in the expanded configuration;

 Figure 11A is a perspective view of yet another alternate embodiment of the vein filter of the present invention shown in the expanded configuration;

 Figure 11B is a view similar to Figure 11A showing an alternate embodiment of the hooks;

30 Figure 11C is a view similar to Figure 11A showing another alternate embodiment of the hooks;

Figure 11D is a view similar to Figure 11A showing yet another alternate embodiment of the filter of the present invention;

Figure 11E is a perspective view of the filter of Figure 11D in the collapsed position;

5 Figure 11F is an enlarged view of the retention hooks of Figure 11D;

Figure 11G is a perspective view of an alternate embodiment of the filter of Figure 7 having the retention hooks of Figure 11D;

Figure 11H is an enlarged view of the retention hooks of Figure 11G in the collapsed position;

10 Figure 12A is a close up perspective view of an alternate embodiment of an end of the filter having a series of cutouts to receive a retrieval snare;

Figure 12B is a close up perspective view of an alternate embodiment of an end of the filter having cutouts to receive a retrieval snare;

15 Figure 12C is a side view of the embodiment of Figure 12B showing a retrieval snare placed in one of the cutouts between the coils;

Figure 13A is a close up perspective view of another alternate embodiment of an end of the filter having a hook to receive a retrieval snare;

Figure 13B is a perspective view of an end of the filter illustrating another alternate embodiment of the hook to receive a retrieval snare;

20 Figures 13C and 13D are perspective and top views, respectively, of an alternate embodiment of the hook to receive a retrieval snare;

Figure 13E is a top view of an alternate embodiment of the hook of Figure 13C;

Figures 13F and 13G are perspective and side views, respectively, of another alternate embodiment of the hook to receive a retrieval snare;

25 Figures 13H-13J are side views showing the method steps for engaging the hook of Figure 13F for removing the filter utilizing a retrieval snare when the snare approaches from one orientation;

30 Figures 13K-13N are side views showing the method steps for engaging the hook of Figure 13F for removing the filter utilizing a retrieval snare when the snare approaches from an orientation opposite the orientation of Figure 13H;

Figures 14, 15 and 16 illustrate delivery and placement of the vessel filter of Figure 1 in the inferior vena cava wherein Figure 14 illustrates initial insertion of the delivery sheath through the femoral vein, Figure 15 illustrates the delivery sheath being advanced toward the inferior vena cava just below (upstream) the juncture of the renal arteries; and Figure 16 illustrates the delivery sheath fully withdrawn to place the filter in the expanded placement configuration in the inferior vena cava;

Figure 17 is a perspective view of one embodiment of a delivery system for the vein filter;

Figure 18 is an exploded view of the delivery system of Figure 17;

Figure 19 is a cross-sectional view showing the engagement of the interlocking rails of the cartridge with the hub;

Figure 20A is a perspective view of an alternate embodiment of the filter of the present invention having interconnecting struts in the filter portion, the filter shown in the expanded configuration;

Figure 20B is a front view of the filter of Figure 20A;

Figure 20C is a side view of the filter of Figure 20A;

Figure 20D is a perspective view of the filter of Figure 20A shown in the collapsed configuration;

Figure 20E is an enlarged view of an end portion of the filter of Figure 20D showing the retention hooks;

Figure 20F is an enlarged developed view of the end portion of the filter of Figure 20D showing the axial relationship of the retention hooks;

Figure 21 is a perspective view of another alternate embodiment of the filter having interconnecting struts in the filter portion;

Figure 22A is a perspective view of another alternate embodiment of the filter of the present invention having interconnecting struts in the filter portion and in the mounting portion;

Figures 22B and 22C are front and side views, respectively of the filter of Figure 22A;

Figure 22D is a perspective view of the filter of Figure 22A shown in the collapsed configuration;

Figure 22E is an enlarged view of an end region of the filter of Figure 22D in the collapsed configuration;

Figure 23 is a perspective view of another alternate embodiment of the vein filter of the present invention in the collapsed configuration for delivery;

5 Figure 24 is a close up perspective view of the retention hooks of the filter of Figure 23 in the collapsed position;

Figure 25 is a perspective view of the vein filter of Figure 23 in the expanded configuration;

Figure 26 is a front view of the filter of Figure 25;

10 Figure 27 is a side view of the filter of Figure 25 showing the axial spacing of the retention hooks; and

Figure 28 is an enlarged developed view of the end portion of the filter of Figure 27.

15 **DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS**

Turning now to the drawings, wherein like reference numerals identify similar or like components throughout the several views, various embodiment of the vein filter of the present invention are described for placement within the inferior vena cava to capture blood clots or other particles which could otherwise pass to the lungs.

20 The filter is movable from a low profile collapsed configuration to facilitate insertion through the delivery sheath to a larger expanded placement configuration to enable atraumatic engagement with the vessel walls to secure (mount) the filter within the inferior vena cava. The filter is preferably substantially bell-shaped and preferably has a flared or mounting region (portion/section) and a filtering region (portion/section). As
25 described in more detail below, the filtering portion has inwardly directed struts, terminating in a converging region, thereby directing particles toward the central axis of the filter. By directing the particles to the center, they will be exposed to greater blood flow which improves dissolution of the particles. The other portion increases in transverse dimension to form a flared region. The flare provides less contact area than a
30 straight region, resulting in less tissue ingrowth to facilitate removal of the filter if

desired. The flare also reduces the chance of vessel distortion if inserted into a curved vena cava.

Turning now to details of the filter of the present invention and with initial reference to Figures 1 and 2, the filter is designated generally by reference numeral 10 and is shown in a collapsed configuration for delivery. Filter 10 is preferably formed from a single tube 11. In a preferred embodiment, the filter 10 is composed of shape memory material, such as Nitinol, a nickel titanium alloy, or elgiloy, however, other materials such as stainless steel are also contemplated. A plurality of cutouts 12 are formed in the filter 10, preferably by laser cutting although other techniques are contemplated. In the illustrated embodiment, six elongated cutouts are formed, creating six strips or struts 14 of substantially uniform width separated by the cutouts 12 and extending from tubular portion 18.

The collapsed configuration of filter 10 reduces the overall profile to facilitate delivery to the site. The diameter or transverse dimension of filter 10 in the collapsed configuration is represented by reference D1 and preferably is about 2mm and more preferably about 1.7mm. Other dimensions are also contemplated. The diameter or transverse dimensions of the filter in the expanded placement configurations (e.g. Figs. 4A and 5) is greater than the diameter or transverse dimension D1 in the collapsed (delivery) configuration. The filter is thus preferably dimensioned for insertion through a 6 French delivery system and through a 6 French catheter.

Figures 3-5 illustrate the expanded placement configuration of the filter 10. Filter 10 is generally bell-shaped in configuration. Filter 10 has a flared region 17 and a converging region 21 at the filtering section 19. The transverse dimension of the filter at flared (or mounting/anchoring) region 17 is thus greater than the transverse dimension at filtering section 19. In larger vessels, the filter can expand to a diameter D2 shown in Figure 5. In smaller vessels, the filter expands to a smaller diameter, e.g. D3, shown in Figure 4. Diameters (or transverse dimensions) D2-D3 preferably range from about 18 mm to about 32mm, depending on the internal diameter of the vessel wall as will be explained in more detail below. Other dimensions are also contemplated.

The elongated struts 14 are spaced apart as shown and extend at an angle away from the longitudinal axis L of filter 10 in region 17 to provide a flare. Preferably, this

angle or taper is about 10° , although other dimensions are contemplated. In the filtering region 19, beginning at an intermediate portion of the filter (the transition between the first and second regions 17, 19) the struts 14 curve or bend inwardly (region 23) toward the longitudinal axis and then extend inwardly at an angle to the tubular portion 18, thereby forming an angle with the longitudinal axis. In the illustrated embodiment, when expanded, the six struts 14 are shown spaced approximately 60 degrees apart. It is also contemplated that a fewer or greater number of struts could be provided and spacing other than 60 degrees be provided.

In the expanded placement configuration, a portion of the each elongated strut 14 has an outer surface 20 for engagement with the vessel wall to retain the filter 10 in position in the vessel. This region is angled with respect to the longitudinal axis. The outer surface 20 of struts 14 could be roughened to enhance engagement. Alternatively, a plurality of atraumatic tabs, barbs or other penetrating members can extend from the outer surface 20 of the struts 14 to engage the vessel wall to retain the filter. Figures 6A and 6B show examples of such retention features. In Figure 6B, the filter has a series of hemispherical cutouts 152 formed along the length of the struts 154 forming pointed edges 156 to engage the vessel wall. The cutouts 152 can be formed along the length of the strut 154 or alternatively be formed only along a portion of the length. The cutouts can also be formed on fewer than all the struts.

In the embodiment of Figure 6A, the filter has anchoring elements 162 formed by cutouts 163 at the ends of the struts 164. Anchoring elements 162 have pointed ends 165. In the collapsed configuration the anchoring elements 162 and their pointed ends 165 are aligned with the struts 164, substantially parallel with the longitudinal axis of the filter to maintain a reduced profile. When the filter moves to the expanded configuration, the pointed ends 165 face outwardly as shown in Figure 6A. Anchoring elements 162 can be placed in the end regions of the strut or in other locations. The anchoring elements can also be placed in the opposite direction shown.

In the embodiment of Figure 11A, the struts 174 of filter 170 terminate in hooks 172 which extend substantially perpendicular from the strut. Hooks extend from the substantially V-shaped region 179 formed by the joining of connecting struts 174a, 174b. In the alternate embodiment of Figure 11C, struts 184 of filter 180 also terminate in

substantially perpendicular hooks 182, however this arrangement is achieved by torquing the connecting struts 184a, 184b at the curved region 185 so the hooks bend out of the plane. As shown, hooks 182 extend from V-shaped region 189 formed by the connecting struts 184a, 184b. In the alternate embodiment of Figure 11B, the hooks 192 of filter 190
 5 (having struts 194) lie in the plane of the connecting struts 194a, 194b, flush with the width surface “w” of the V-shaped region 199 of connecting struts 194a, 194b.

In the alternate embodiment of Figures 11D-11F, the hooks 302 lie in the same plane as the connecting struts 304a, 304B of struts 310 as in Figure 11B; however the hooks of filter 301 are of two different sizes. More specifically, a first set of hooks 302a
 10 is larger than a second set of hooks 302b. Preferably when formed in a laser cut tube, hooks 302a are formed so that they occupy a region equivalent to the transverse dimension of two adjacent struts. For example, in the collapsed configuration, hook 302a occupies a region (dimension) of four connecting struts while smaller hook 302b would only occupy the region (dimension) of two connecting struts. Smaller hooks 302b are
 15 spaced axially inwardly with respect to larger hooks 302a to minimize the collapsed profile (transverse dimension) of the filter when collapsed for insertion. In this preferred embodiment, smaller hooks 302b occupy the space created by the larger hooks 302a so they can be considered as nesting within larger hooks 306a. Stated another way, each hook 302b has an outer surface 307 which conforms (follows the contour) to an inner
 20 surface 309 of a hook 306a. The penetrating tips 306a, 306b in hooks 302a, 302b, respectively, penetrate the tissue to retain the filter, preferably temporarily.

The aforescribed hooks 172, 182, 192, 302 (as well as the hooks described below) can be used with any of the disclosed embodiments (see e.g. Figure 11G). Such hooks can also be formed or placed on fewer than all the struts.

25 Referring back to Figures 3-5, the filter portion of filter 10 will now be discussed. As noted above, the filtering section of filter 10 at a first end of the filter is designated generally by reference numeral 19 and includes the converging region 21. Filtering section 19 extends from the flared region 17, and extends toward the central longitudinal axis L of the filter 10 and converges at portion 32 into tubular portion 18. At the
 30 transition region between the filtering and flared regions 19, 17, struts 14 bend inwardly (region 23), then extend radially inwardly toward the tubular portion 18, and transition to

the tubular portion 18. The tubular portion 18 and converging region 19 of the filter 10 are spaced both axially outwardly and radially inwardly from the bend regions 23 of the strut 14. (Axially outwardly is represented by arrow "a" and radially inwardly is represented by arrow "b" in Figure 4A). The filter is designed to direct particles to the center of the filter and vessel. (Trapping the particles at the center rather than the edges of the filter is more desirable because there is less blood flow at the edges of the vessel and greater blood flow at the center to better dissolve the particles.) For clarity, not all of these sections of each strut 14 are labeled in the drawings, it being understood that the non-labeled struts can have the same configurations.

Turning now to the flared or mounting (anchoring) region 17, each strut 14 is divided into two connecting strut portions 14a, 14b. Preferably, each strut portion 14a, 14b is about one half the width of the undivided strut 14, although other widths are contemplated. The strut portions 14a, 14b of each divided strut 14 extend in opposite directions and include a curved region 25 as the strut portions 14a, 14b each extend toward respective strut portion 14a or 14b of an adjacent strut. That is, strut portions 14a, 14b form connecting portions to connect adjacent struts 14 as connecting strut 14a of one strut is connected to connecting strut 14b of an adjacent strut. Connecting strut portion 14a on one strut and portion 14b of another strut converge at end region 29 of the filter and form a substantially V-shaped region. Six such V-shaped end portions are preferably formed, each portion connecting adjacent struts. Note that although all six struts 14 are shown interconnected, it is also contemplated that fewer than all the struts can be interconnected.

Note the designations of longitudinal, angled, curved, bowed, connected, joined, interconnected, connecting strut, etc. in the illustrated embodiments refer to the same integral strut and are divided into such regions for ease of understanding.

It should be understood that the elongated struts 14 bend as they move from their collapsed position to their expanded placement configuration. Therefore, stated another way, the filter 10 can be viewed as having a filtering section 19 at a first end extending from the tubular portion 18. As viewed, each of the struts 14 emerges from the tubular portion 18 at an angle that extends outwardly away from the center to transition to curved portions 23. The curved portions 23 extend outwardly away from the longitudinal axis

forming a flare or region of progressively increasing transverse dimension. In this flared region 17, near a second end of the filter (opposite the end containing tubular portion 18), the struts 14 are interconnected by connecting struts 14a, 14b that curve inwardly toward the connecting strut 14a or 14b of an adjacent strut to form a substantially V-shaped end
5 portion.

In the placement (expanded) configuration, the filter 10 moves towards its memorized position and the extent it returns to its fully memorized position will be dependent on the size of the vessel in which the filter 10 is inserted. (The larger the vessel, the closer the filter comes to returning to it's fully memorized position). This can
10 be understood by comparing Figures 4A and 5 which illustrate by way of example two possible expanded dimensions of the filter; Figure 4A showing expansion to a smaller dimension occurring in smaller diameter vessels and Figure 5 showing expansion to a larger dimension occurring in larger diameter vessels.

To enable movement between an expanded and collapsed configuration, the filter
15 tube of the embodiments described herein is preferably made of shape memory metal material, such as Nitinol, a nickel titanium alloy. The memorized configuration of the filter 10 is shown in Figure 1. To facilitate passage of the filter 10 through the lumen of the delivery sheath 100 (shown in Figure 14 in conjunction with the method of insertion) and into the vessel, cold saline can be injected into the delivery sheath or catheter 100 and
20 around the filter 10 in its collapsed position within the delivery sheath 100. This shape memory material characteristically exhibits rigidity in the austenitic state and more flexibility in the martensitic state. The cold saline maintains the temperature dependent filter 10 in a relatively softer condition as it is in the martensitic state within the sheath. This facilitates the exit of filter 10 from the sheath 100 as frictional contact between the
25 filter 10 and the inner surface of the sheath would otherwise occur if the filter was maintained in a rigid, i.e. austenitic, condition.

Once ejected from the delivery sheath or catheter 100, the filter is no longer cooled and is exposed to the warmer body temperature, which causes the filter 10 to return towards its austenitic memorized configuration.

The filter 10 (and other filters described herein) can be inserted through the jugular vein in the neck of the patient or through the femoral vein in the leg of the patient or the arm. The filters can also be placed in the superior vena cava.

Figures 14-16 illustrate delivery and placement of the filter 10, by way of example, in the inferior vena cava. Delivery catheter 100 is inserted through the femoral vein "f" and advanced through the iliac arteries into the inferior vena cava. Delivery catheter would be withdrawn once the tip of the sheath is adjacent the structure so that withdrawal of the sheath would place the filter in the desired location of Figure 16. Tubing 104 and valve assembly 106 enable saline injection. Delivery catheter 100 is withdrawn to enable filter 10 to be warmed by body temperature to transition to the expanded placement configuration. The other filters described herein could be inserted in the same manner. Note it is implanted in the orientation such that filter section 19 is downstream of the flared section 17. This enables blood clots or other particles to be directed to the center of the filter section by the angled struts. Thus the direction of insertion, e.g. upstream or downstream direction, will determine how the filter is to be positioned in the delivery catheter.

In an alternate embodiment of the filter, the strut width can vary. For example, the struts can be wider at the flared region than at the filtering portion. This is preferably achieved by removing material to create the thinner portions. These thinner portions increase the flexibility of the filter for forming the angled and curved portions upon deployment. Alternatively, the filter can have struts which are thinner, rather than wider, at the flared region, than at the angled and curved regions of the filtering portion. This would provide more stability at the curved regions. The adjustment of the widths is designed to strike a balance between stability and flexibility of the various regions of the filter. Thus, other width variations are contemplated such as making multiple width changes within each strut and/or in different struts.

Figures 7-9 illustrate an alternate embodiment of the filter, designated by reference numeral 110. Filter 110 is similar to filter 10 except for end region 121. That is, like filter 10, filter 110 has a filtering region 119 which extends from the flared (anchoring/mounting) region 117, and extends toward the central longitudinal axis L of the filter 110 and converges at portion 132 into tubular portion 118. Struts 114 bend

inwardly toward the longitudinal axis of the filter 10 at region 123. For clarity, not all of these sections of each strut 114 are labeled in the drawing, it being understood that the non-labeled struts can have the same configurations. The flared region 117 as in filter 10 is of an angle preferably about 8 degrees although other angles are contemplated.

5 The end region 121 of filter 110 where the struts 114 interconnect differs from filter 10. In filter 110, the struts 114 are interconnected by connecting strut portions 114a, 114b that curve outwardly away from the central axis and then inwardly toward each other to form a substantially V-shaped end portion 127. At the outward curved or bowed portion 124, the connecting struts are joined to connecting struts of adjacent struts
10 114 (region 125). Thus, a closed geometric shape 133 is formed as shown. The closed shape as shown is substantially oval in configuration, although other shapes are contemplated. Six such closed geometric shapes are preferably formed, each connecting adjacent struts, although fewer closed shapes are contemplated if fewer than all the struts are interconnected. Also, the length of the region 125 where the struts are joined can be
15 shorter or longer than that shown, thereby changing the configuration of the closed geometric shape (e.g. making it longer or shorter).

 Stated in other words, each strut 114 divides into two connecting strut portions 114a, 114b which initially extend outwardly from each other. As each strut extends outwardly, the strut portion 114a joins the strut portion 114b of an adjacent strut at region
20 125. After this joined region 125, the strut portions 114a and 114b which emanate from the same strut extend inwardly towards each other and are joined at their ends into a substantially V-shaped end, designated by reference numeral 127.

 The collapsed configuration of filter 110 is shown in Figure 9 with cutouts 112 forming six struts 114. Regions 113 illustrate where struts 114 divide.

25 In the alternate embodiment of Figure 10, filter 150 resembles filter 10 of Figure 1 except for the additional connecting struts or ribs 152. These ribs increase the stability of the filter 150. As shown, the two ribs 152 extend from adjacent struts 154 and curve inwardly towards each other and are joined at region 156 (forming a V-like connection). The ribs 152 can be arranged so they are axially aligned as in Figure 10 or alternatively
30 can be staggered i.e. spaced axially (not shown). Also, the ribs can be placed between fewer than all the struts and the ribs can be utilized with any of the foregoing

embodiments. Note that the ribs are preferably integrally formed with the filter, formed by the laser cutting process mentioned above; however, alternatively the ribs can be attached to the struts. Struts 154 divide into connecting struts 154a, 154b in the embodiment of Figure 1.

5 Figures 11G and 11H illustrate an alternate embodiment of the filter of Figure 7 having the hooks of filter 301 of Figure 11D. Filter 350, like filter 110, has struts 354 which are interconnected by connecting strut portions 354a, 354b that curve outwardly then inwardly toward each other to form V-shaped portions 357, terminating in hooks 356. As in Figure 11D, large hooks 356a alternate with axially offset smaller hooks 356b
10 and are identical to hooks 306a, 306b of Figure 11D.

In another embodiment, the ribs could curve radially outward near their tips, thus contacting the vessel wall and acting as a retaining mechanism.

Figure 20A illustrates an alternate embodiment of the filter of the present invention. In this embodiment, the struts are interconnected at the filtering region rather
15 than at the flared mounting (anchoring) region. This creates closed geometric shapes at the filtering region to enhance the clot capturing capability of the filter. Also, by providing the interconnection more forward (downstream) in the filter, i.e. in the filtering region (filtration zone), linear movement of the filter is facilitated to enhance removal of
the filter.

20 Turning first to Figures 20A and 20C, bell-shaped filter 700 has a filtering region 719 and a flared anchoring (mounting) region 721 of greater transverse dimension. Flared region 721 is preferably at an angle of about 8 degrees to about 14 degrees with respect to the longitudinal axis of the filter, although other angles are contemplated. In this flared region 721, the transverse dimension increases towards the anchoring end of
25 the filter 700 so that as in the other embodiments disclosed herein, the terminal end of the filter at region 719 has a smaller transverse dimension than at the opposing terminal end at region 721. The filtering region 719 extends from the flared region 721 toward the longitudinal axis of the filter 700 and converges at portion 732 into tubular portion 718 at
the filter end portion of filter 700.

30 Filtering region 719 has six struts 714 curving outwardly from tubular portion 718. Each filter strut or strut portion 714 extends radially from tubular portion 718 and

divides into two connecting filter struts or strut portions 714a, 714b (preferably of equal width) that angle away from each other (in different directions) to extend to the connecting strut portion of an adjacent strut 714. Thus, connecting strut portion 714a of one strut 714 interconnects with the connecting strut portion 714b of an adjacent strut at joining region 714d. This forms closed geometric shapes 725, preferably substantially diamond shaped in configuration. For clarity, not all of the identical parts are labeled in the drawing. In the illustrated embodiment, preferably six struts are provided forming twelve interconnecting struts, however a different number of struts and closed geometric shapes can be provided. Also, fewer than all of the struts could be interconnected. Although preferably the struts 714 divide into connecting struts 714a, 714b of half the width, other dimensions are contemplated.

After convergence of strut portions 714a, 714b at joining region 714d, it transitions into elongated mounting strut portions 714c which form flared mounting or anchoring region 721. The length of the strut portions 714c in the anchoring region 721 can vary, with increased/decreased length increasing the flexibility/rigidity of the struts. The thickness of the strut portions can also vary to affect flexibility/rigidity.

In one embodiment, the strut portions 714c terminate in hooks 740a, 740b similar to hooks 302a, 302b of Figure 11D. That is, hooks 740a and 740b lie in the plane of the struts 714c and hooks 740a are larger than hooks 740b, formed so they occupy a region equivalent to the transverse dimension of two adjacent struts. Smaller hooks 740b nest within larger hooks 740a as described above in conjunction with hooks 302a, 302b. Note that smaller hooks 740b are spaced axially (inwardly) of hooks 740a as well as spaced axially with respect to each other as represented by the arrows in Figure 20F designating the three different distances E1, E2 and E3 in the developed view, presented for ease of understanding since the hooks are formed from a tube. Other hook designs could alternatively be provided, including the various hook embodiments described herein.

The tubular portion 718 is preferably in the form of a retrieval hook as described herein with respect to the other embodiments, and preferably in the form of retrieval hook 290 of Figure 13F. Other retrieval structure can also be utilized.

In the alternate embodiment of Figure 21, the filter is designated generally by reference numeral 800 and has a filtering region 819 and a flared anchoring (mounting)

region 821. The filter 800 differs from filter 700 in the additional joining regions of the connecting struts. More specifically, filter struts 814 extend radially from tubular portion 818, in a similar manner as struts 714 of Figure 20A. Struts 814 divide into connecting struts or strut portions 814a, 814b, extending in different directions, and then join at first joining regions 814c to a connecting strut of an adjacent strut 814. Emanating from joining regions 814c, connecting struts or strut portions 814f, 814g, extend in different directions, away from each other, to connect to another adjacent strut 814f or 814g at second joining regions 814d. At regions 814d, the mounting struts or strut portions 814h extend longitudinally to form the flared mounting or anchoring region 821. The interconnecting struts preferably form a first set of substantially diamond shaped closed geometric shapes 830 as shown and a second set of substantially hexagonal shaped closed geometric shapes 832. Other shapes are contemplated as are a different number of struts 814, interconnecting struts, and closed geometric shapes. For clarity, not all identical parts are labeled in the drawings.

At the terminal ends of the struts 814 at the mounting portion 821, retention hooks are provided. Hooks 840a, 840b as shown are identical to hooks 740a, 740b of Figure 20. Retrieval hook 850 at the tubular end portion 818 of the filtering end portion of filter 800 is preferably identical to retrieval hook 750 of filter 700. Other hook designs and retrieval structure could alternatively be utilized.

Figures 23-28 illustrate an alternate embodiment of the filter of the present invention, designated generally by reference numeral 1010. Filter 1010 is substantially identical to filter 700 of Figures 20A-20E except for the retention hooks. Filter 1010 has struts interconnected in the filtering region and not in the flared mounting (anchoring) region as in filter 700. This creates closed geometric shapes at the filtering region to enhance the clot capturing capability of the filter. The mounting region is devoid of such closed geometric shapes as it is devoid of interconnecting or connecting struts. This facilitates removal.

Filter 1010 is substantially bell shaped and has a filtering region 1012 and a flared anchoring (mounting) region 1024 of greater transverse dimension. Flared region 1024 is preferably at an angle of about 8 degrees with respect to the longitudinal axis of the filter, although other angles are contemplated. In this flared region 1024, the transverse

dimension increases towards the anchoring end of the filter 1010 so that as in the other embodiments disclosed herein, the terminal end of the filter at region 1019 has a smaller transverse dimension than at the opposing terminal end at region 1021. The filtering region 1012 extends from the flared region 1024 toward the longitudinal axis of the filter 1010 and converges at portion 1022 into tubular portion 1018 at the filter end portion of filter 1010.

Filtering region 1019 preferably has six struts 1014 curving outwardly from tubular portion 1018. Each filter strut or strut portion 1014 extends radially from tubular portion 1018 and divides into two connecting (interconnecting) filter struts or strut portions 1014a, 1014b (preferably of equal width) that angle away from each other (in different directions) to extend to the connecting strut portion of an adjacent strut 1014. Thus, connecting strut portion 1014a of one strut 1014 interconnects with the connecting strut portion 1014b of an adjacent strut at joining region 1014d. This forms closed geometric shapes 1025, preferably substantially diamond shaped in configuration, although other shapes are contemplated. For clarity, not all of the identical parts are labeled in the drawing. In the illustrated embodiment, preferably six struts are provided forming twelve interconnecting struts, however a different number of struts and closed geometric shapes can be provided. Also, fewer than all of the struts could be interconnected. Although preferably the struts 1014 divide into connecting struts 1014a, 1014b of half the width, other dimensions are contemplated.

After convergence of strut portions 1014a, 1014b at joining region 1014d, it transitions into elongated mounting strut portions 1014c which form flared mounting or anchoring region 1024. The length of the strut portions 1014c in the anchoring region 1024 can vary, with increased/decreased length increasing the flexibility/rigidity of the struts. The thickness of the strut portions can also vary to affect flexibility/rigidity.

Preferably, the strut portions 1014c terminate in hook portions 1030. Hook portions 1030 in this embodiment are preferably of substantially the same size. In the preferred embodiment, the hook portions or the struts from which they extend have different lengths so that the distalmost end of the hook portions 1030 terminate at different axial positions. Stated another way, the hooks are staggered in an axial direction so the struts terminate at different points. Figure 28 illustrates the six different

distances, in the developed view, presented for ease of understanding since the hooks are formed from a tube.

Hook portions 1030 lie in the plane of a distal portion 1014d of the struts 1014c. That is, the distal portion 1014d of the strut 1014c twists out of the plane of the remaining portion of the strut, with the hooks lying in the plane of the distal portion.

Hook portions 1030 includes a hook 1032 having a penetrating tip 1034 preferably pointing toward a proximal portion (filter region) of the filter 1010. A top wall 1036 of the hook 1032 has a slight step 1038. The penetrating tip 1034 extends about a curved wall 1039. The penetrating tip 1034 in the illustrated embodiment extends substantially parallel to a longitudinal axis L1 of the struts portion 1050. Opposite the curved wall 1039 on hook 1032 are a plurality of teeth 1040, with points or edges facing in a distal direction, opposite the direction of the penetrating tip 1034. Teeth 1040 engage the vessel wall to provide additional retention to prevent movement of the implanted filter in the caudal direction. A heel 1044 is formed on a distal end of the hook portion 1030, terminating in a curved surface 1046 and extending distally beyond the hook 1032. Heel 1044 extends past the hook 1032 to function as a stop to prevent the filter strut portions from going through the vessel wall. Hook portion 1030 also has a reduced width dimension Z1 which transition from the strut 1014d to the hook 1032. For clarity, only some of the hooks and hook portions are labeled in Figure 28.

Preferably hook portions 1030 somewhat nest within an adjacent hook portion. More specifically, the strut of portion 1030 has a reduced area 1049 (with width dimension Z1) which forms a gap 1045 to receive a portion of heel 1044 of an adjacent hook portion 1030. In this configuration, a portion of the heel 1044 of the hook portion 1030 is in general longitudinal alignment with a penetrating tip 1034 of an adjacent hook as described below.

The strut 1014d at the reduced area portion 1049 has a first wall 1052 and a second wall 1054 forming a width Z1 defined as the distance or space between the walls 1052, 1054. The strut 1014d adjacent the reduced area 1049 has a first wall 1056 and a second wall 1058, forming a width Z2, defined as the distance or space between walls 1056, 1058. Line S1 represents this first wall 1056 of strut 1014d. As can be appreciated, the hook 1032 has a height Z3 greater than height Z2 such that it extends widthwise

beyond the height of the first wall 1052. In other words, the penetrating tip 1034 extends radially beyond the Line S1, illustrated by line S2 (extrapolated from the penetrating tip 1034). By way of example, width Z1 could be between about .013 inches to about .019 inches, and preferably about .016 inches, width Z2 could be between about .025 inches to about .035 inches, and preferably about .030 inches, width Z3 could be about .035 inches to about .045 inches, and preferably about .040 inches, and width Z4 at the heel 1044 could be between about .011 inches to about .017 inches, and preferably about .014 inches. It should be understood that other dimensions are also contemplated.

Line S3 represents the second wall 1058 extrapolated in a proximal direction. As can be appreciated, the heel 1044 extends widthwise beyond the line S3 and width of the second wall 1054. Wall 1058 also includes a slight indentation 1055 to accommodate the penetrating tip portion 1034 of the adjacent hook 1032.

The tubular portion 1018 is preferably in the form of a retrieval hook as described herein with respect to the other embodiments, and preferably in the form of retrieval hook 290 of Figure 13F. Other retrieval structure can also be utilized.

Figure 22 illustrates an alternate embodiment of the filter of the present invention. In this embodiment, the struts are interconnected at the filtering region (filtration zone) and at the flared mounting (anchoring) region. These interconnecting struts at the filtering region enhance the clot capturing capability of the filter. The interconnection at the mounting region enhances the stability of the filter and the vessel retention capability by reducing the flexibility of the struts.

Referring to Figures 22A and 22C, bell-shaped filter 900 has a filtering region 919 and a flared anchoring (mounting) region 921 of greater transverse dimension. Flared region 921 is preferably at an angle of about 8 degrees with respect to the longitudinal axis of the filter, although other angles are contemplated. In this flared region 921, the transverse dimension increases towards the anchoring end of the filter 900 so the terminal end of the filter at region 919 has a smaller transverse dimension than the opposing terminal end at region 921. The filtering region 919 extends from the flared region 921 toward the longitudinal axis of the filter 900 and converges at portion 932 into tubular portion 918 at the filter end portion of filter 900.

Filtering region 919 has six struts 914 curving outwardly from tubular portion 918. Each elongated filter strut or strut portion 914 extends radially from tubular portion 918 and divides into two connecting filter struts or strut portions 914a, 914b (preferably of equal width) that angle away from each other (in different directions) to extend to the
5 connecting strut portion of an adjacent strut 914. Thus, connecting strut portion 914a of one strut 914 interconnects with the connecting strut portion 914b of an adjacent strut at joining region 914d. This forms closed geometric shapes 925, preferably substantially diamond shaped in configuration. For clarity, not all of the identical parts are labeled in the drawing. In the illustrated embodiment, preferably six struts are provided forming
10 twelve interconnecting struts in the filtering region, however a different number of struts and closed geometric shapes can be provided. Also, fewer than all of the struts could be interconnected. Although the struts 914 can divide into connecting struts 914a, 914b of half the width, other dimensions are contemplated such as equal to the width.

After convergence of strut portions 914a, 914b at joining region 914d, it
15 transitions into elongated mounting strut portions 914c which form flared mounting or anchoring region 921. The length of the mounting strut portions 914c in the anchoring region 921 can vary, with increased/decreased length increasing the flexibility/rigidity of the struts. The thickness of the strut portions can also vary to affect flexibility/rigidity. Each strut 914c divides into two connecting mounting strut portions 914e, 914f. Each
20 strut portion 914e, 914f can be one half the width of the undivided strut 14, although other widths are contemplated such as equal to the width. The strut portions 914e, 914f of each divided strut 914c extend in opposite directions and include a curved region as the strut portions 914e, 914f each extend toward respective strut portion 914e or 914f of an adjacent strut. That is, strut portions 914e, 914f form connecting portions to connect
25 adjacent struts 914c as connecting strut 914e of one strut is connected to connecting strut 914f of an adjacent strut. Connecting strut portion 914e on one strut and portion 914f of another strut converge at end (joining) region 929, as closed geometric shapes 935 are formed. End region 929 has an elongated region (or hook strut) 931 and preferably terminates in hooks described below. Note that although all six mounting struts 914 are
30 shown interconnected, it is also contemplated that fewer than all the struts can be interconnected.

Thus, as can be appreciated, the elongated struts have a first angled region of interconnecting (connecting) struts 914a, 914b in the filtering region 919 and a second angled region of interconnecting (connecting) struts 914e, 914f in the mounting region 921. The region of the interconnecting struts in the first region (the filtering region) has a transverse dimension less than the transverse dimension of the region having the interconnecting struts in the mounting region.

In the embodiment of Figure 22, the filter strut portions and mounting strut portions each divide into connecting struts of half the width. In an alternate embodiment, the filter struts and mounting struts are also bifurcated, however the width of the connecting strut is increased so it is greater than one half the width of the struts and can for instance be equal to the width of the strut. Such bifurcation with increased width is also applicable to the other embodiments of the filter described herein. Bifurcation with decreased width is also contemplated.

Preferably, the strut portions 914c terminate in hooks 940a, 940b similar to hooks 302a, 302b of Figure 11D. That is, hooks 940a and 940b lie in the plane of the struts 914 and hooks 940a are larger than hooks 940b, formed so they occupy a region equivalent to the transverse dimension of two adjacent struts. Smaller hooks 940b nest within larger hooks 940a in the same manner as described above in conjunction with hooks 302a, 302b. Note that smaller hooks 940b are spaced axially (inwardly) of hooks 940a as well as spaced axially with respect to each other in the same manner as described with respect to hooks 740b of filter 700 and illustrated in Figure 20F showing the three different distances E1, E2 and E3 in the developed view. Other hook designs could alternatively be provided, including the various hook embodiments described herein.

The tubular portion 918 is preferably in the form of a retrieval hook 950 as described herein with respect to the other embodiments, and preferably in the form of retrieval hook 290 of Figure 13F. Other retrieval structure can also be utilized.

Filters 700, 800 and 900 are preferably manufactured from a cut tube, preferably laser cut. Therefore, as in the other embodiments described herein, terms such as interconnected, connected, joined, etc., are used for ease of description, it being understood that preferably these portions are integral as they are preferably formed from a single tube. Also, mounting struts and filter struts used to describe the various

embodiments disclosed herein can be considered as mounting strut “portions” or “sections” and filter strut “portions” or “sections” of the same struts if the filter is formed integrally, e.g. from a cut tube.

The foregoing filters can be inserted through the femoral vein or alternatively
5 through the internal jugular vein. It can be removed from access through the internal jugular vein or femoral vein. Various methods can be used to remove the filter such as those described in commonly assigned co-pending application serial no. 09/911,097, filed July 23, 2001, now published application 2002-0193827-A1, published December 19, 2001, including for example, slotted hooks, graspers, etc. A recess or cutout can also be
10 provided at the tubular end portions to receive a snare or other device for removal. A hook 222 at tubular portion 220 is illustrated in the embodiment of Figure 13A and is configured to receive a snare. Figure 13B illustrates another embodiment of a hook. Hook 232 formed in tubular portion 230 forms a cutout 234 for receiving a snare or other removal device. The snare can surround and grasp both ears 235. However, the gap 237
15 between the ears 235 also enables a retrieval snare to lie in the gap 237 to surround and grasp one of the two ears 235.

In the alternate embodiment of Figures 13C and 13D, hook 272 is similar to hook 232 of Figure 13B in that it has two ears 275 with a gap 277 therebetween. However it differs in that it has a bottom cutout 278 formed between walls 279. It also differs in that
20 surfaces 274 of ears 275 are rounded and outer proximal walls 278a angle outwardly (proximally) to curved peak 276 then angle inwardly (wall 278b) to provide a smoother transition into the retrieval sheath. Thus, two angled transitions are provided.

In the alternate embodiment of Figure 13E, to further enhance the transition to facilitate withdrawal into the retrieval sheath, the side walls 284 extending into ears 285
25 of hook 282 angle inwardly toward the longitudinal axis. Consequently, there are three angled transitions: 1) an angled transition in a first direction formed by angled walls 288a which angle proximally outwardly from the edge 285a of ears 285 to the curved peak 285b (the proximal end of the hook is designated generally by reference numeral 283); 2) an angled transition in a second direction formed by angled walls 288b which angle
30 distally outwardly from curved peak 285b; and 3) an angled transition formed by walls 284 which angle proximally inwardly as walls 284 come closer together toward the

proximal end. This results in a smoother transition into the retrieval sheath as it reduces the likelihood of the filter proximal end, i.e. the hook, being caught on the edge of the sheath – the angled edges which create camming surface for all approaches of the filter (360 degree range) will help the hook edges slide into the sheath.

5 Figures 13F and 13G illustrate another alternate embodiment of the retrieval hook of the present invention. This is the retrieval hook shown in conjunction with filter 301 of the embodiment of Figures 11D and 11G. Hook 290 has a curved hook 292 at the proximalmost end. This hook 292 is configured to receive a retrieval snare or other
10 interior surface 294. That is, being formed from a laser cut tube, a wall portion is removed to expose curved inner wall surface 294. This annular interior surface 294 extends from radiused region 295 to proximalmost edge 296. The interior surface 294, for ease of explanation, can be considered to have an interior surface 294a at the radiused
15 region 295 and an interior surface 295b at the hook 292. The interior surface 294b accommodates a portion of a tubular snare sheath. That is, the outer wall of the snare sheath (tube) can partially fit within the cut out region 293. This enhances removal as the snare pulls the filter hook into collinear arrangement with the sheath tube. This can be appreciated by reference to Figures 13H-13J discussed below. The radiused region 295,
20 spaced axially (distal) from the hook 292, includes a radiused or curved edge defined by radiused side walls 297a, 297c and top wall 297b. The angled side walls 297a, 297c form camming surfaces to direct the hook 290 and filter into the retrieval sheath. This can be appreciated by reference to Figures 13K-13N discussed below.

It should be appreciated, that the hook can be formed in other ways to provide an interior annular surface to function in a similar manner as surface 294, i.e. to receive the
25 snare tube.

It should be appreciated that any of the retrieval hooks can be used with any of the filters described herein.

In Figures 13H-13J, the snare approaches the retrieval hook 290 in the orientation shown. This results in a collinear arrangement. More specifically, the snare 502 is part
30 of a retrieval system which includes a snare sheath or tube 504 through which the snare 502 extends. The distal wall 503 of snare sheath 504 provides for cinching of the snare

502. The snare sheath 504 is inserted through retrieval sheath 510. When the filter is pulled into the retrieval sheath 510 it is collapsed for removal. As discussed above, preferably cold saline is injected during the removal process to cool the sheath to transition to a softer martensitic state to facilitate removal.

5 In the orientation shown, as snare 502 retracts the filter, the snare sheath 504 fits into the cut out region 293 as its outer wall conforms to the inner wall surface 294b of hook 292. Thus, the hook 290 and snare sheath 504 become substantially collinear as shown in Figure 13I. This collinear arrangement facilitates retraction into the retrieval sheath 510 as it reduces the likelihood of a wall of the hook getting caught on the distal
10 edge 512 of the retrieval sheath 510, thus providing a smoother transition into the sheath as shown in Figure 13J.

 Figures 13K-13N illustrate the retrieval steps when the snare approaches from the opposite orientation of Figure 13H, i.e. below the hook as viewed in the orientation of Figure 13K. As the snare 502 retracts the filter towards the sheath 510, the wall 297b
15 contacts the edge 512 of retrieval sheath 510 and due to the radiused walls 297a, 297c (depending on the side of contact), the hook is cammed downwardly (in the orientation of Figure 13M) into the retrieval sheath 510 as shown in Figure 13N. This provides a smooth transition into the retrieval sheath 510 as it reduces the likelihood of the hook being caught on the sheath edge.

20 Figure 12A illustrates another embodiment having a series of recesses 210 along the length of the tubular portion 212. This enables the tubular portion 212 to be grasped at several locations along its length, facilitating grasping of the filter for removal. These multiple recesses or cutouts 210 are axially spaced as shown. In the embodiment of Figure 12B, the end of the tubular portion 240 has a series of axially spaced cutouts 242
25 which form a coil-like engagement structure. This engagement structure provides multiple engagement areas for a retrieval (removal) device, such as a retrieval snare, for grasping the filter as the device can for instance be cinched in any of the spaces (formed by the cutouts) between the turns 246 in the helical coil. Figure 12C shows a snare 300 placed in one of the cutouts 242.

30 To facilitate removal of the filter from the vessel, cold saline can be injected onto the implanted filter to change the temperature of the filter to move it to a relatively softer

condition to facilitate the filter being drawn in to the retrieval sheath. That is, injection of cold saline will cause the filter to approach its martensitic state, bringing the filter to a more flexible condition. The flexible condition facilitates the collapse and withdrawal of the filter into the retrieval sheath, by decreasing the frictional contact between the filter and the inner surface of the retrieval sheath.

A delivery system for the filter of the present invention is shown in Figures 17 and 18. The delivery system 600 includes a hub 602, a cartridge 604 containing the filter, a pusher 606 and a wire 608 extending through the pusher 606. The wire 608 extends through the cartridge 604 and through the length of tube 603 to maintain a separation of the hooks, e.g. hooks 402 of filter 350 of Figure 11G, during insertion of the delivery system and delivery of the filter. The cartridge 604 is removably attached to the hub 602, preferably by a snap-fit although other modes of attachment are also contemplated. The cartridge preferably has markings (not shown) on the outer surface to indicate a femoral or jugular direction so the user knows the orientation to attach the cartridge 604 to hub 602.

Once attached, advancement of the pusher 604 advances the filter from the cartridge and through tube 603 as the distal edge of the pusher 604 abuts the proximal end of the filter, with the wire 608 (e.g., a Nitinol wire) preventing entanglement of the retention hooks. The wire 608 also provides support (stability) for the pusher 604 as the pusher 604 is advanced over the wire 608. The filter is forced out of the distal end of the tube, where it is no longer cooled by saline and is warmed by body temperature to return toward its memorized configuration.

To enhance the retention of the cartridge 604 in the hub 602, a locking mechanism can be provided such as the mechanism of Figure 19. The cartridge 604 has a pair of locking rails 612a, 612b, each including a respective recess 614a, 614b. The hub 602 contains a detent 620 as shown. When the cartridge 604 is inserted into the hub 602, the recess 614a of the locking rails 612a is retained by the detent 620. This locks the cartridge 604 to the hub 602 during use, preventing unwanted separation of the cartridge 604 from the hub 602. If access via the jugular artery instead of the femoral artery is desired, then the cartridge is inserted so that recess 614b of rail 612b engages detent 620 of hub 602.

While the above description contains many specifics, those specifics should not be construed as limitations on the scope of the disclosure, but merely as exemplifications of preferred embodiments thereof. For example, the filters can be inserted in other regions of the body. Also, any of the aforescribed filters can have mounting sections of varying thickness. The foregoing filters can be made of materials other than shape memory material. Those skilled in the art will envision many other possible variations that are within the scope and spirit of the disclosure as defined by the claims appended hereto.

CLAIMS:

1. A vessel filter comprising a first region and a second region, the filter movable between a collapsed position for delivery to the vessel and an expanded position for placement within the vessel, the first region having a filter portion having a converging region to direct particles toward the center of the filter, the first region including a plurality of spaced apart filter struts, the struts each having a first width defined as a distance between a first wall and a second wall and having a longitudinal axis, a plurality of hooks at the second region, the hooks having a vessel penetrating tip and a heel, the penetrating tip of one hook longitudinally aligned with a portion of the heel of an adjacent hook.
2. The vessel filter of claim 1, wherein the hooks have a third and fourth wall and a second width defined between the first and second walls, the width of the hook being greater than the first width of the strut from which it extends such that the penetrating tip portion of the hook extends radially beyond the first wall.
3. The vessel filter of claim 1 or 2, wherein the heel of the hooks extends radially beyond the second wall of the strut.
4. The vessel filter of any one of claims 1 to 3, wherein each of the struts has a reduced diameter area extending longitudinally along the strut and transitioning into the hook, the reduced diameter area providing a space to accommodate the heel of an adjacent hook.
5. The vessel filter of any one of claims 1 to 4, wherein the penetrating tip of the hooks points in a proximal direction toward the first region and the heel extends in an opposite direction.
6. The vessel filter of any one of claims 1 to 5, wherein the heel of the hooks has a third width less than the first width of the respective strut.

7. The vessel filter of any one of claims 1 to 6, wherein the heel extends at an angle to the longitudinal axis.
- 5 8. The vessel filter of any one of claims 1 to 7, wherein a top portion of the hook is axially aligned with an inward curve in a wall of an adjacent hook portion.
9. The vessel filter of any one of claims 1 to 8, wherein a top portion of the hook has a stepped surface, the hooks have a curved end surface.
- 10 10. The vessel filter of any one of claims 1 to 9, wherein the hook includes a series of teeth, and one of the teeth is substantially aligned with an axis passing through a penetrating tip of the hook.
- 15 11. The vessel filter of any one of claims 1 to 10, wherein the hook includes a series of teeth, the teeth extending from a non-linear surface.
12. The vessel filter of any one of claims 1 to 11, wherein the heel terminates in a curved surface and a portion of the curved surface is longitudinally aligned with the first
20 wall of the strut.
13. The vessel filter of any one of claims 1 to 12, wherein the hooks include a plurality of teeth, the penetrating tip extending in a first proximal direction toward the first region and the teeth extending in a second different distal direction, the penetrating
25 tip and teeth preventing movement of the filter in opposing directions.
14. The vessel filter of any one of claims 1 to 13, wherein an end of the penetrating tip extends substantially parallel to the longitudinal axis of the strut.
- 30 15. The vessel filter of any one of claims 1 to 14, wherein the heels of adjacent vessel engaging hooks terminate axially spaced.

FIG-1

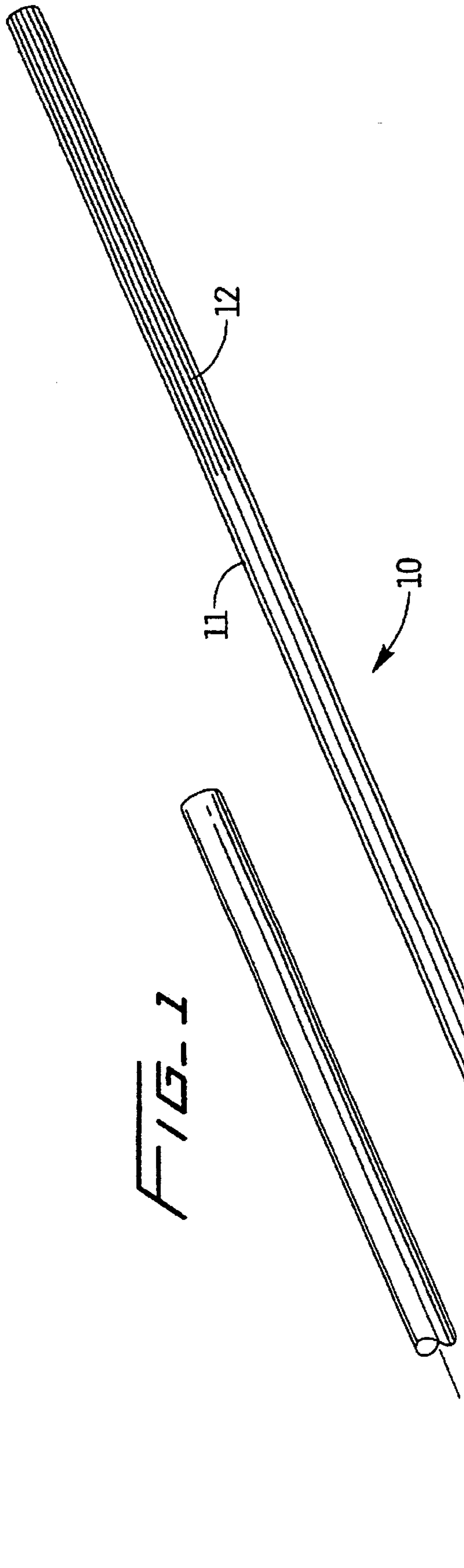
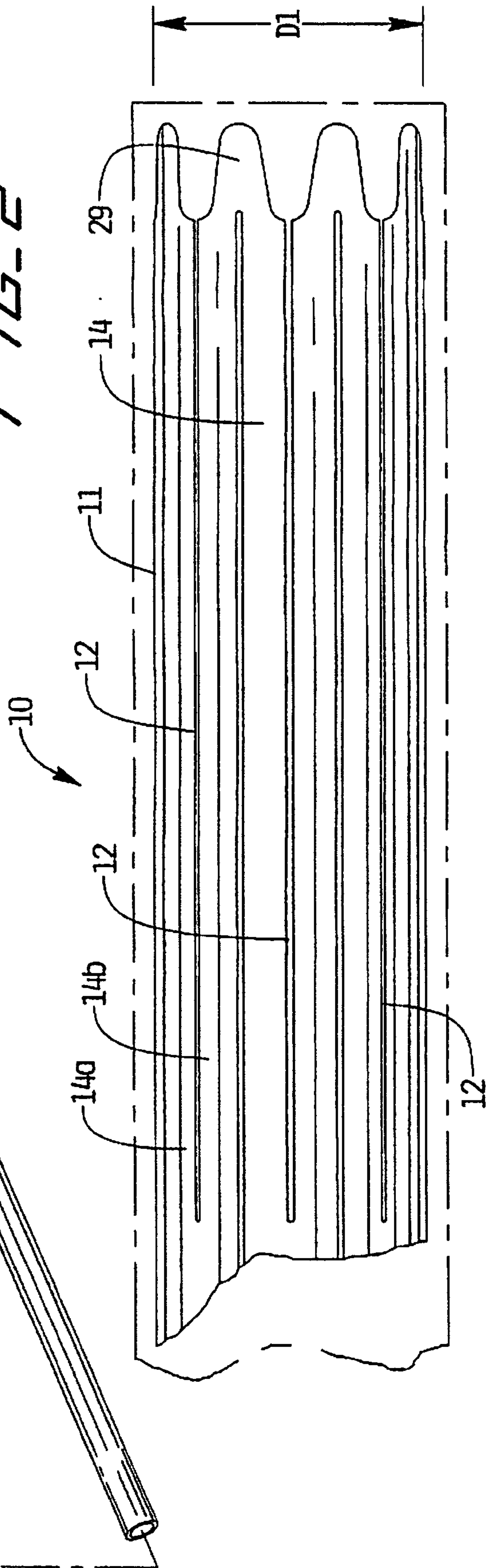


FIG-2



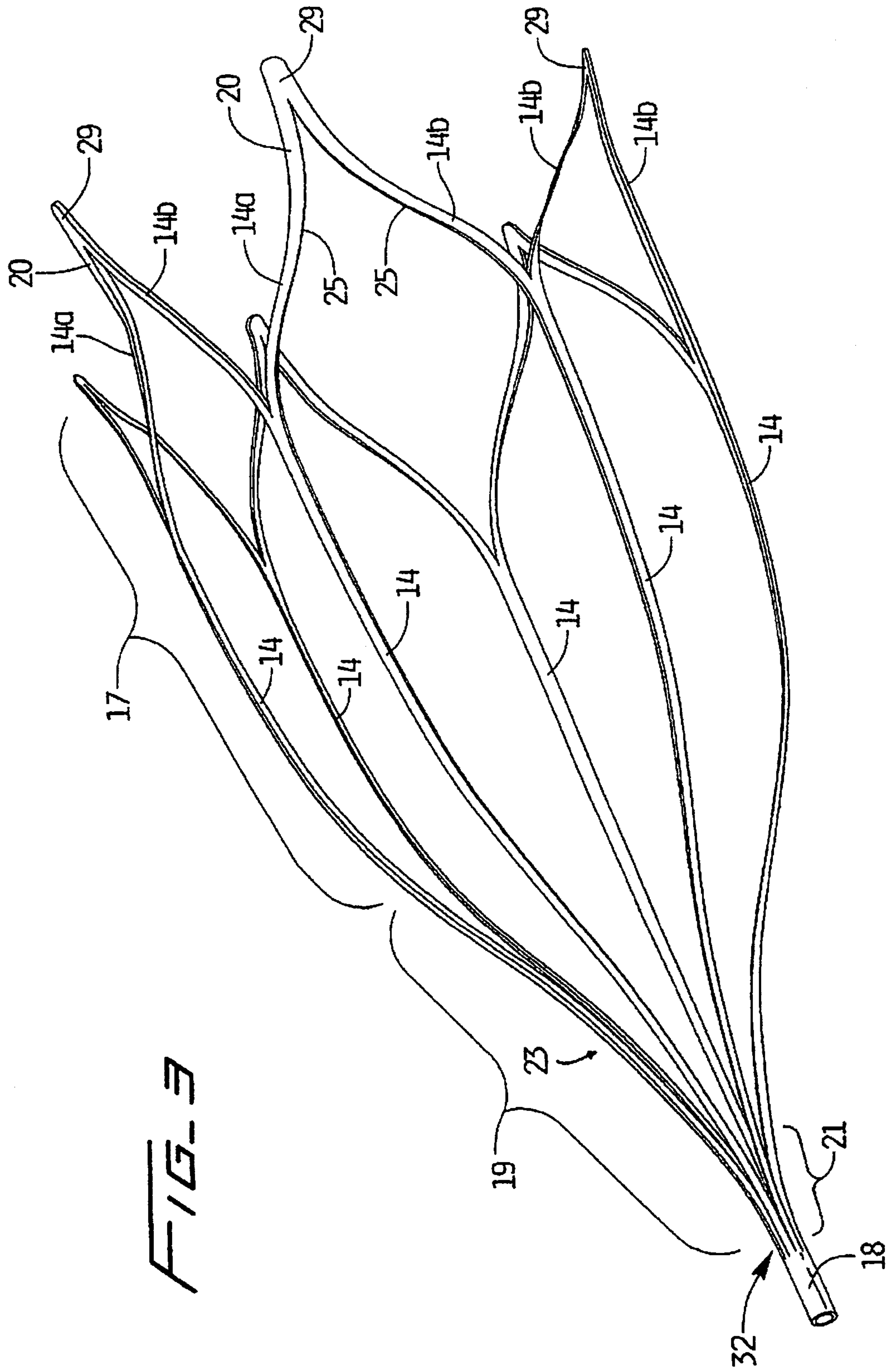


FIG. 3

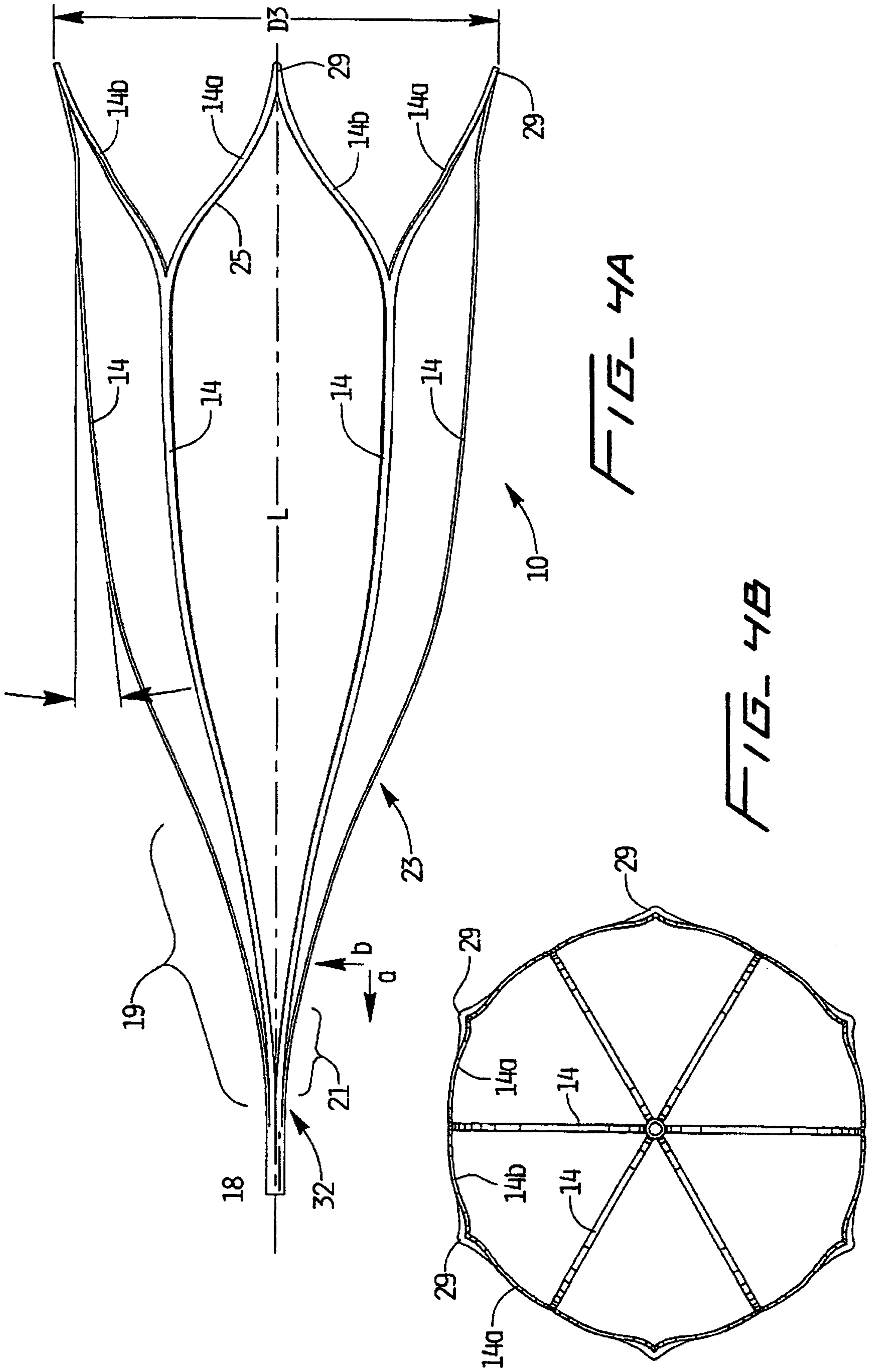


FIG. 4A

FIG. 4B

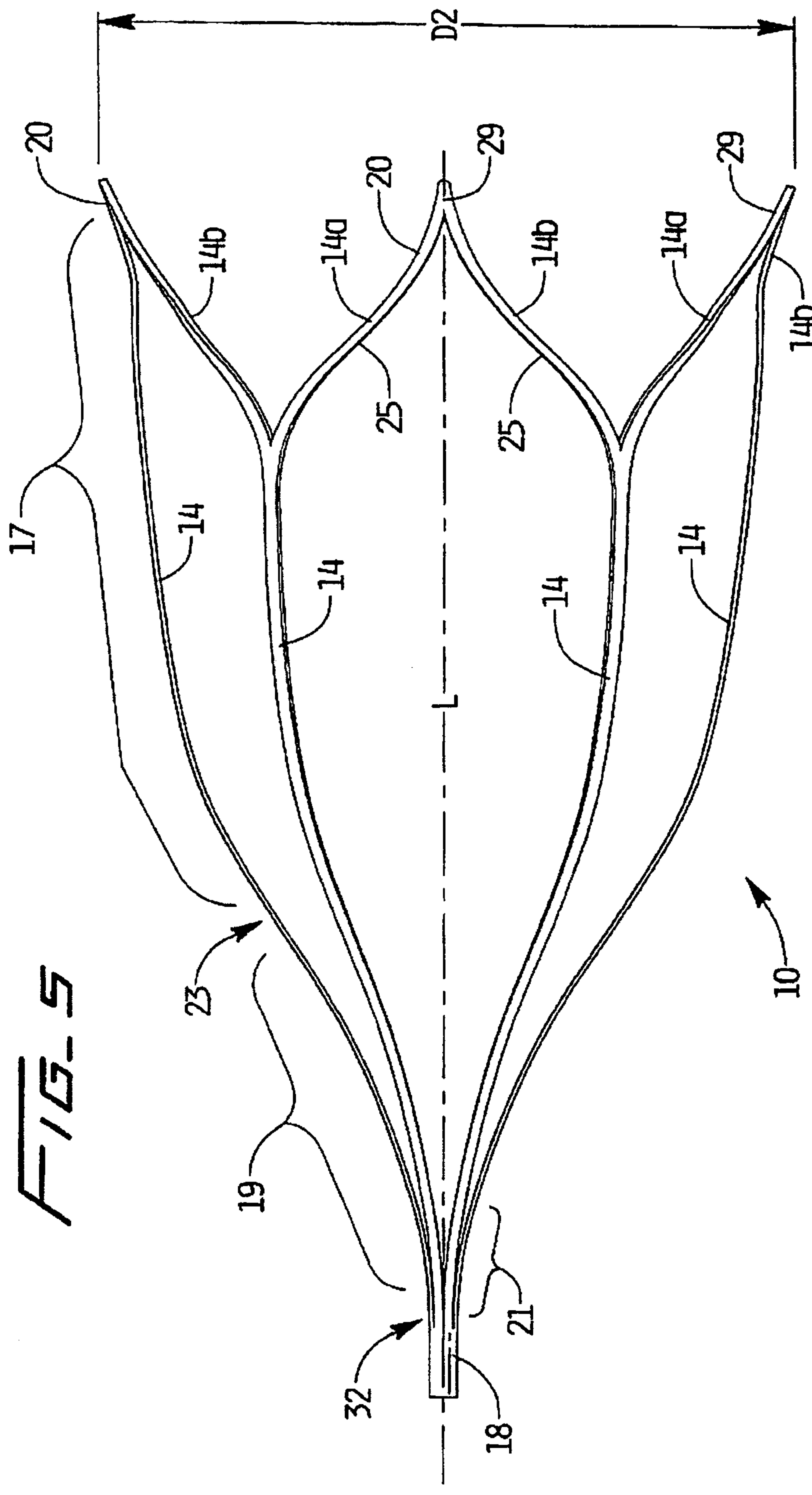


FIG. 6A

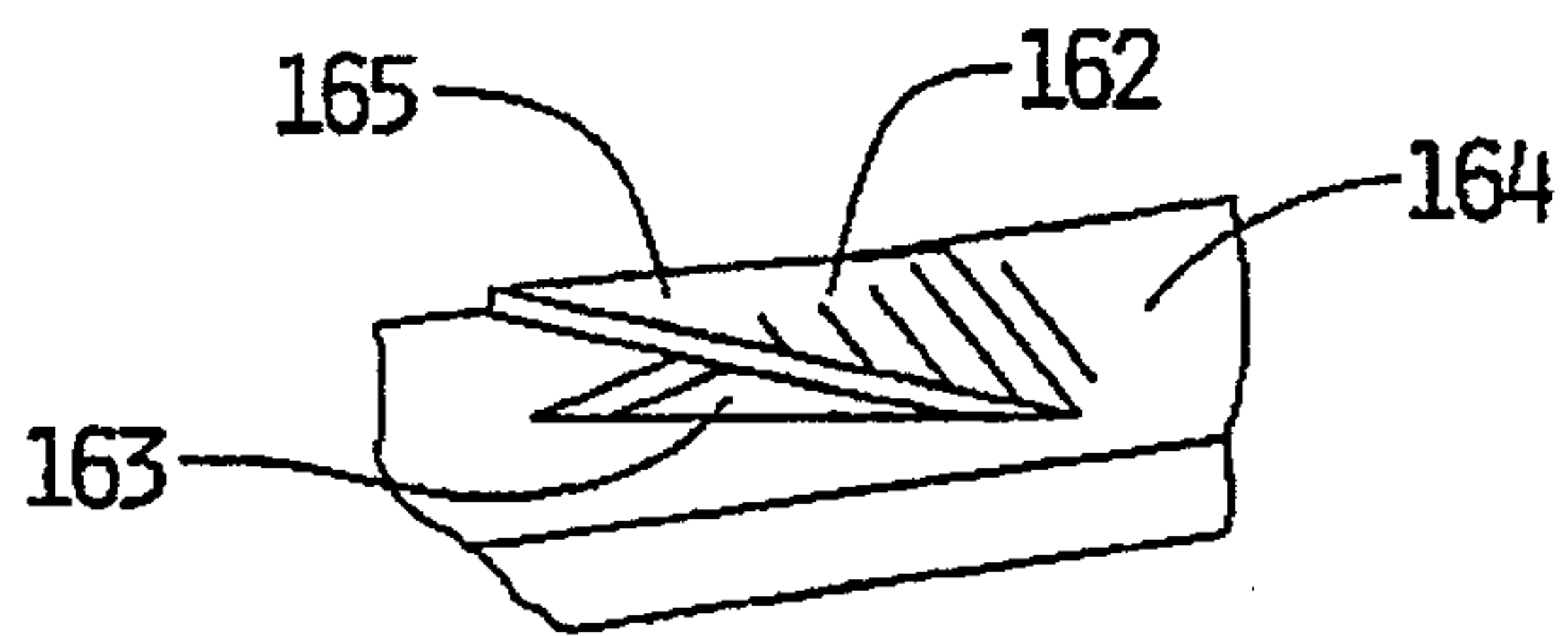
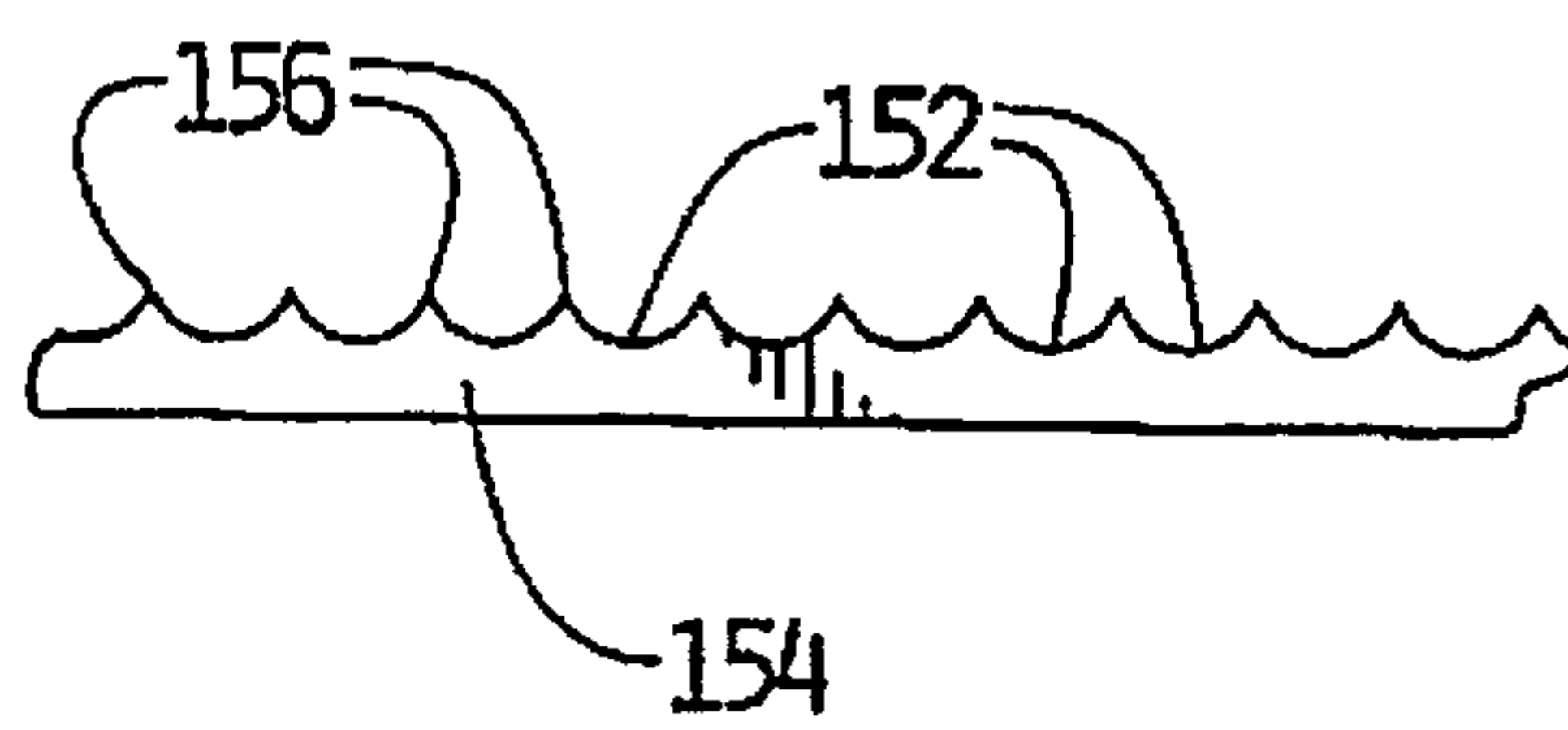
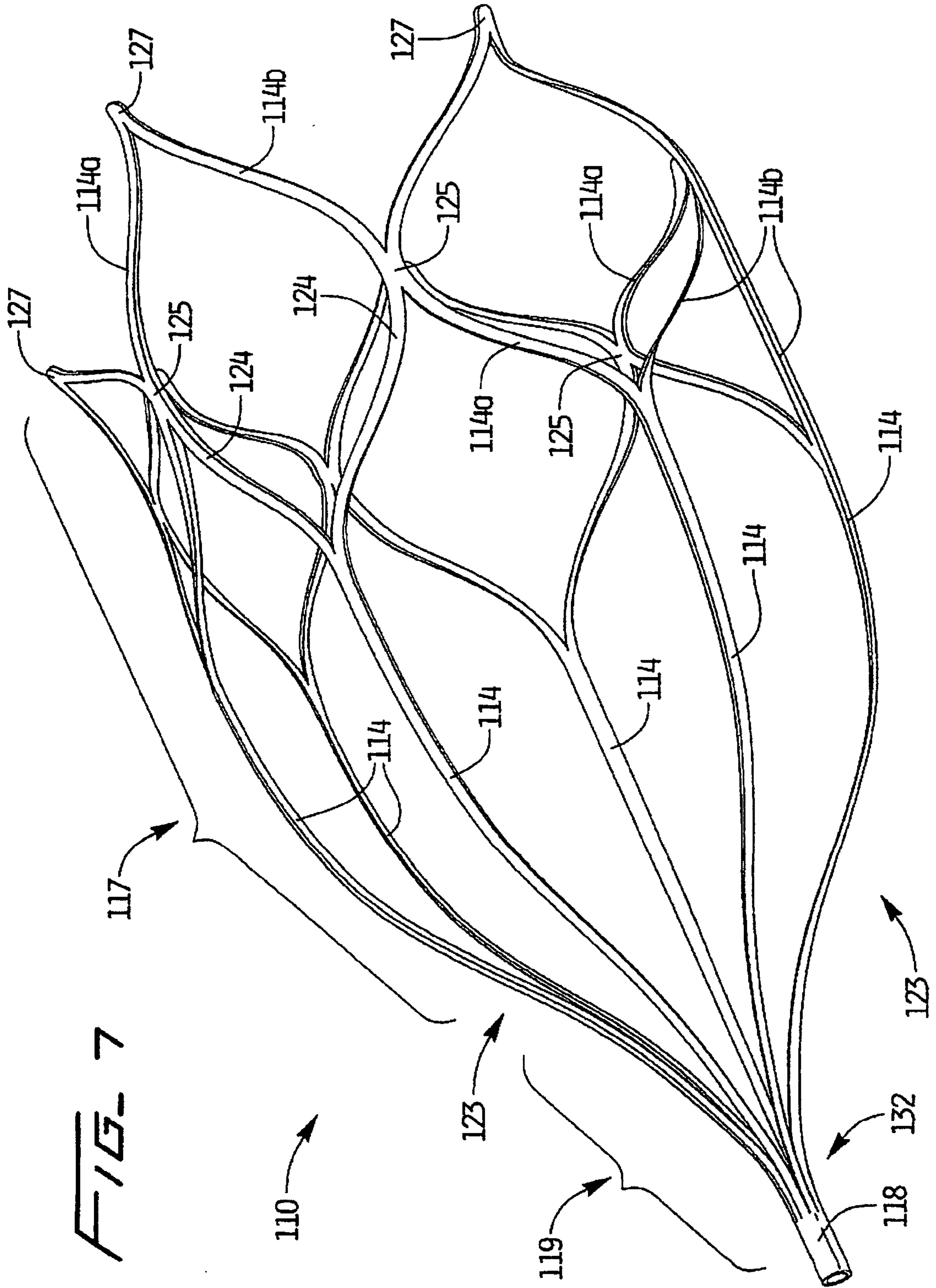
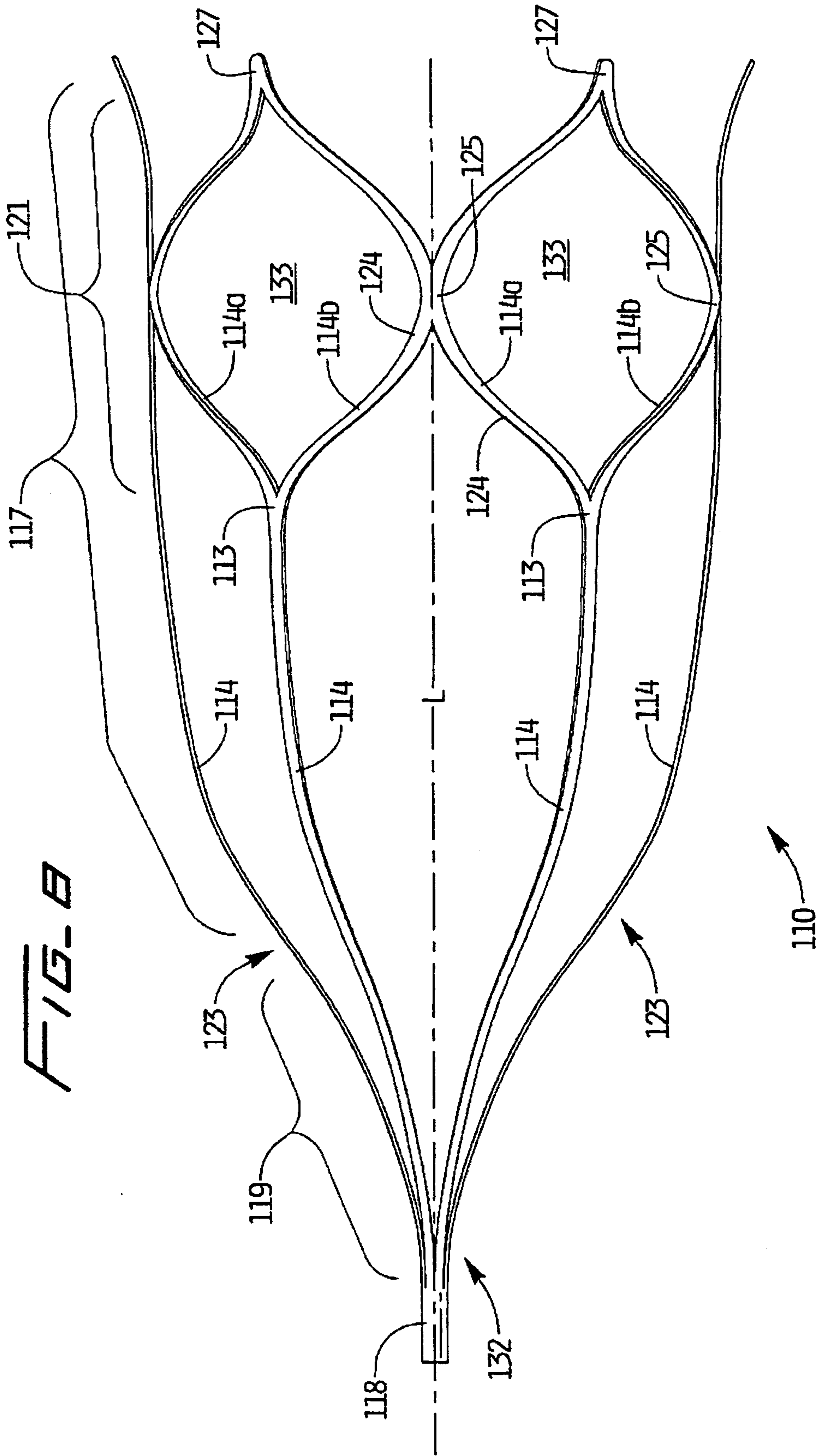


FIG. 6B







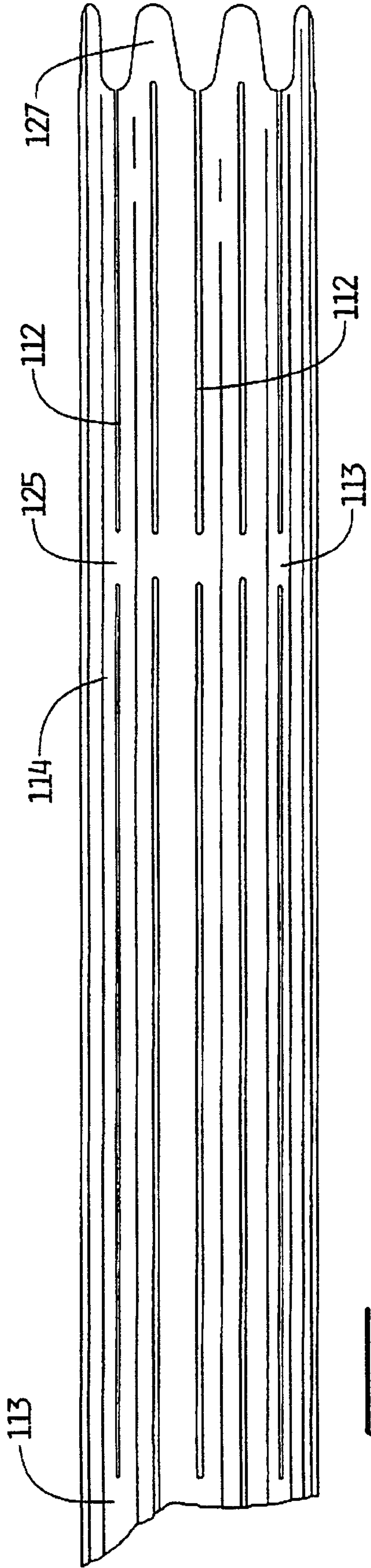


FIG. 9

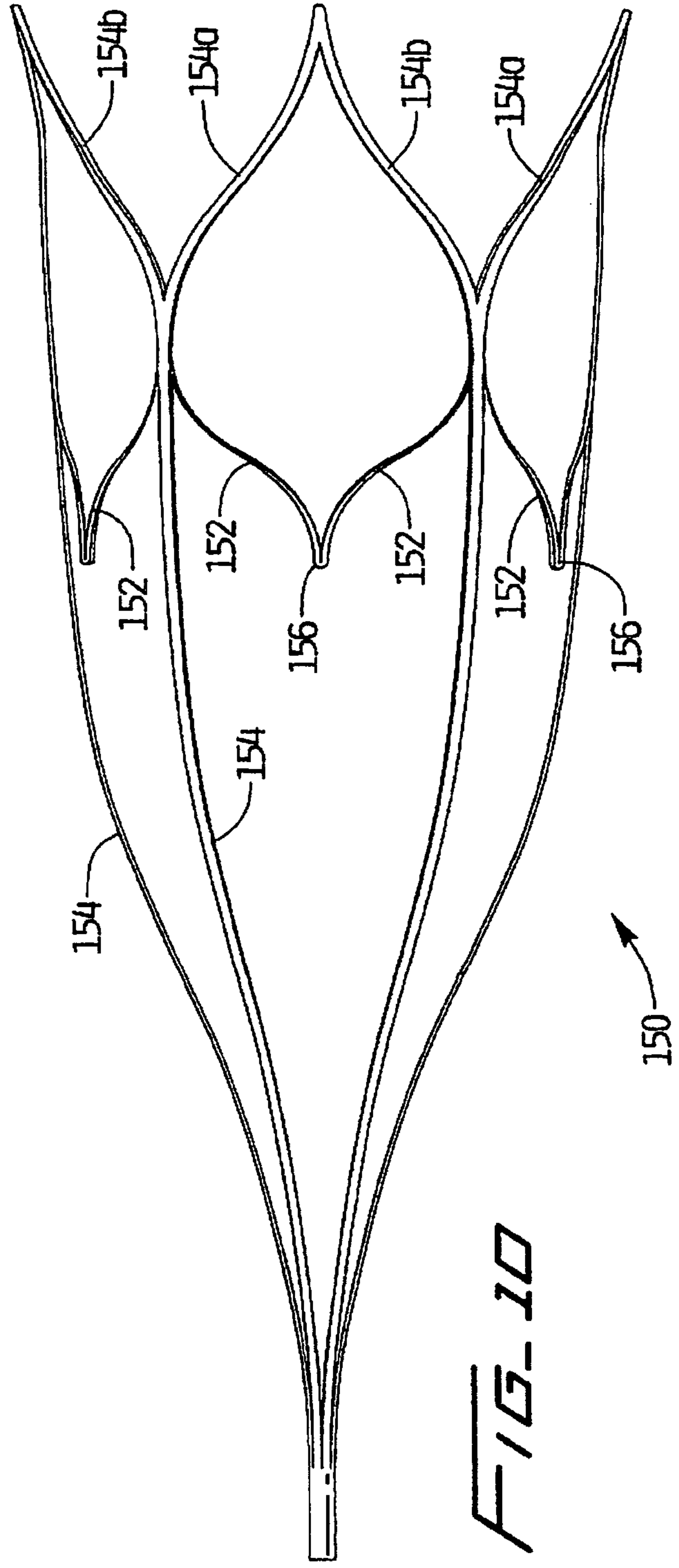


FIG. 10

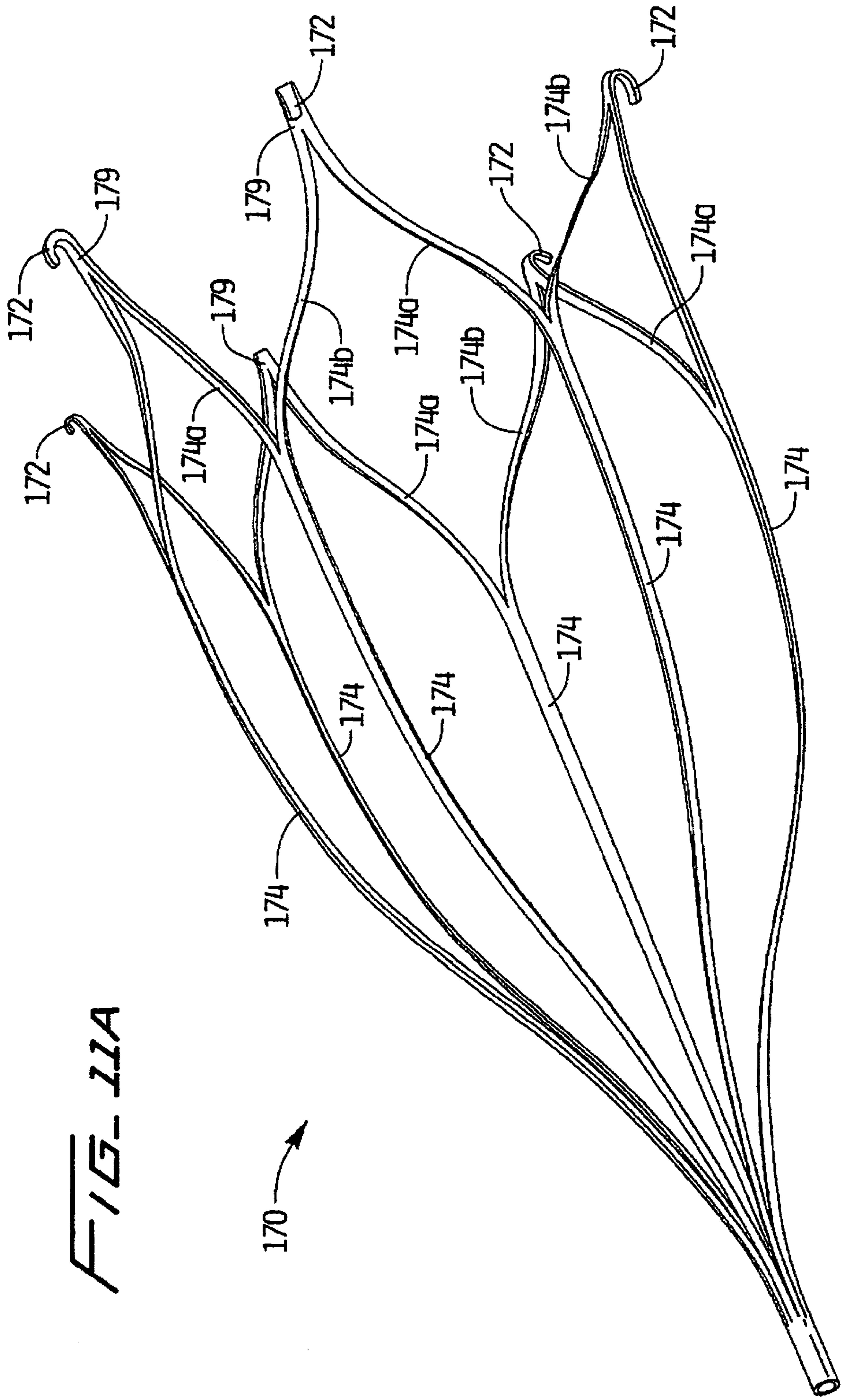


FIG. 11A

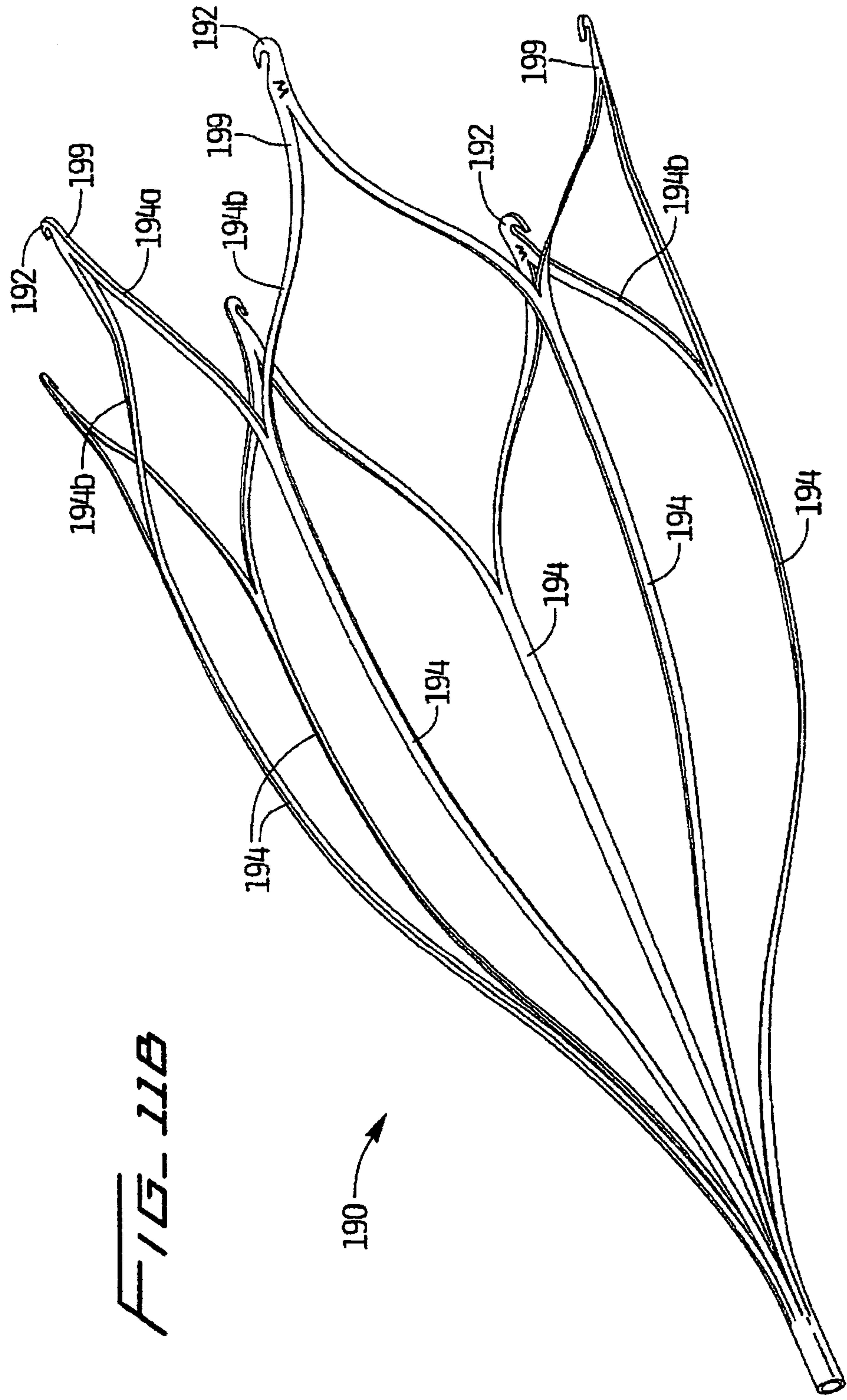


FIG. 11B

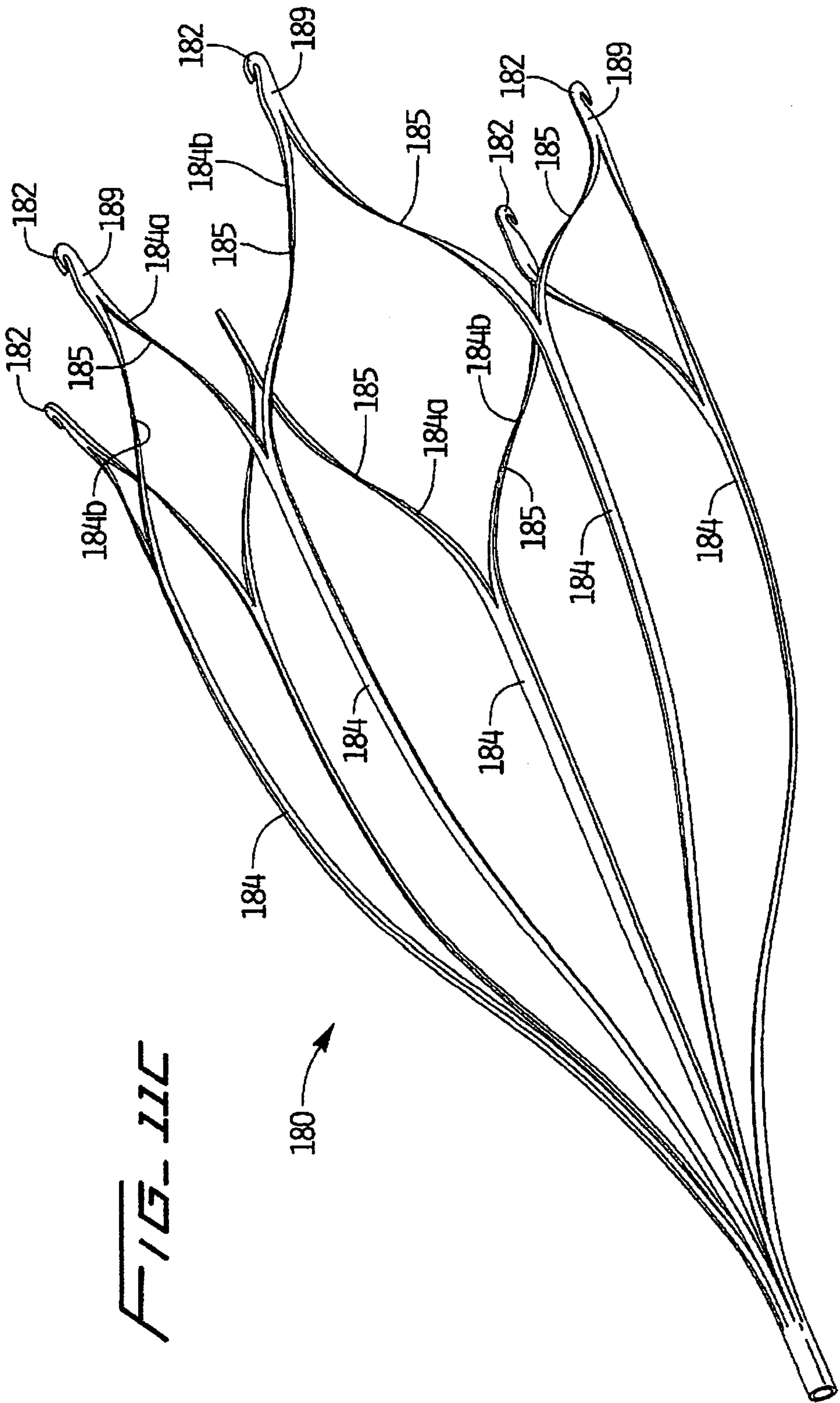


FIG. 11C

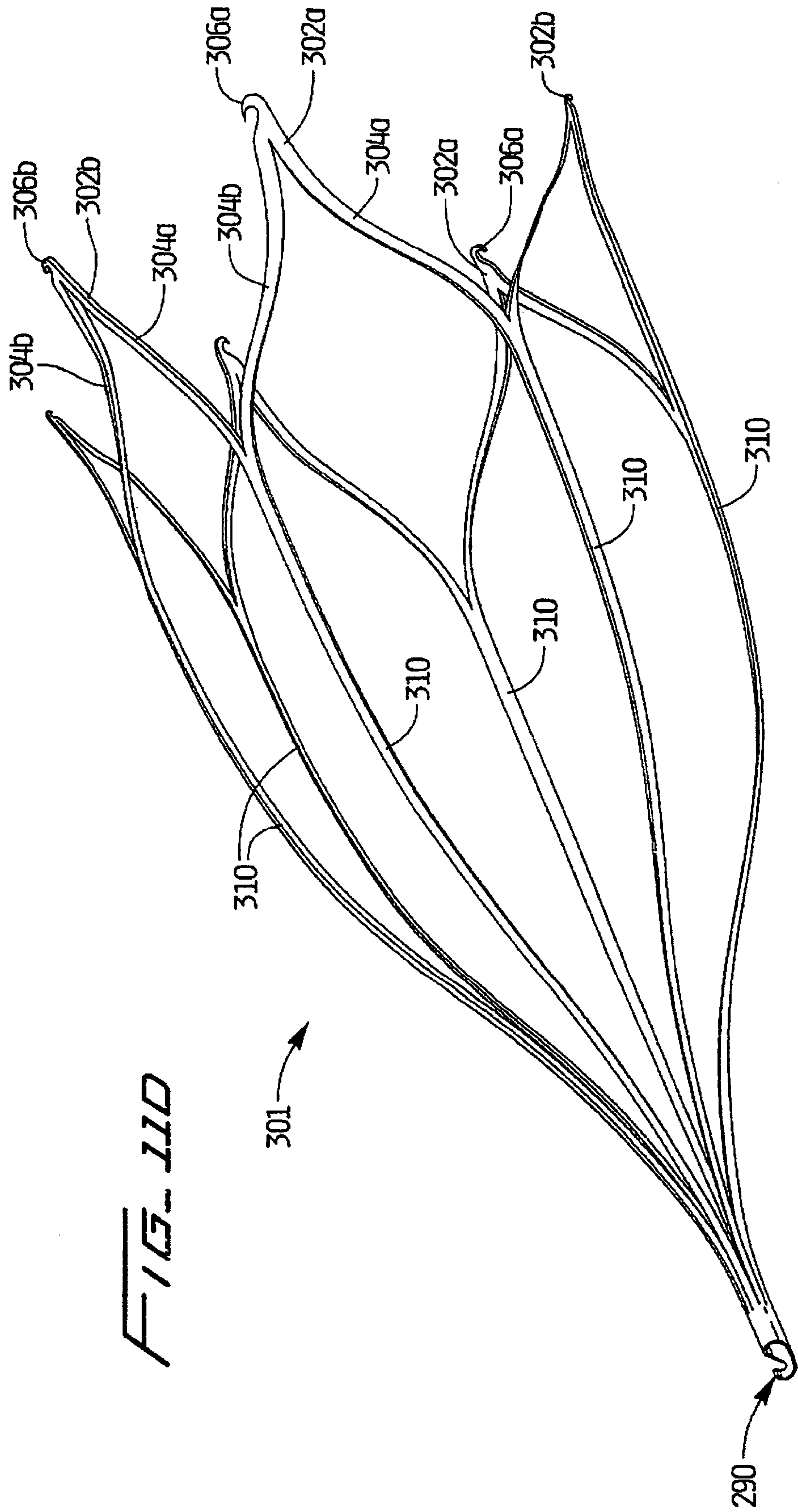


FIG. 110

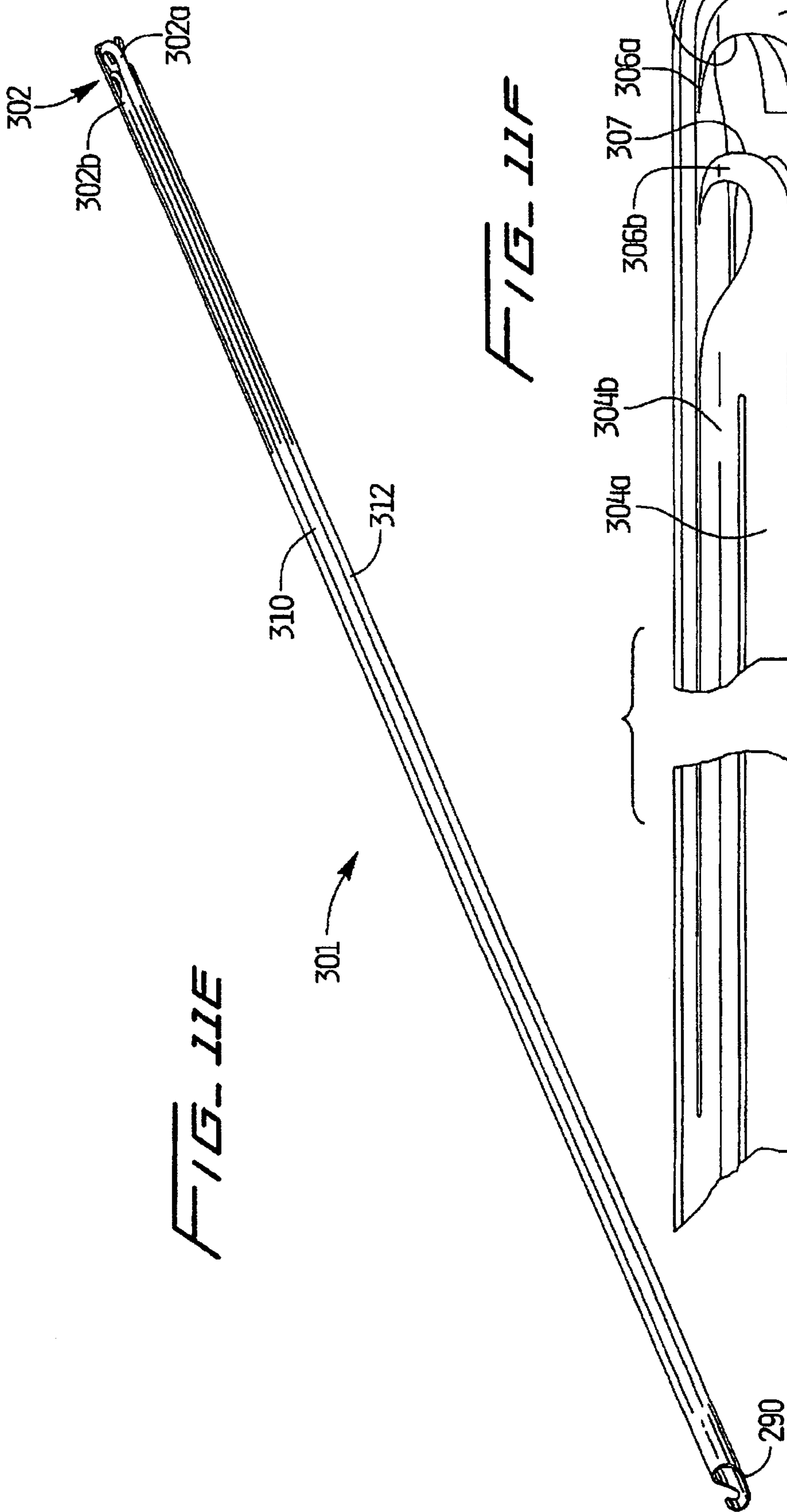
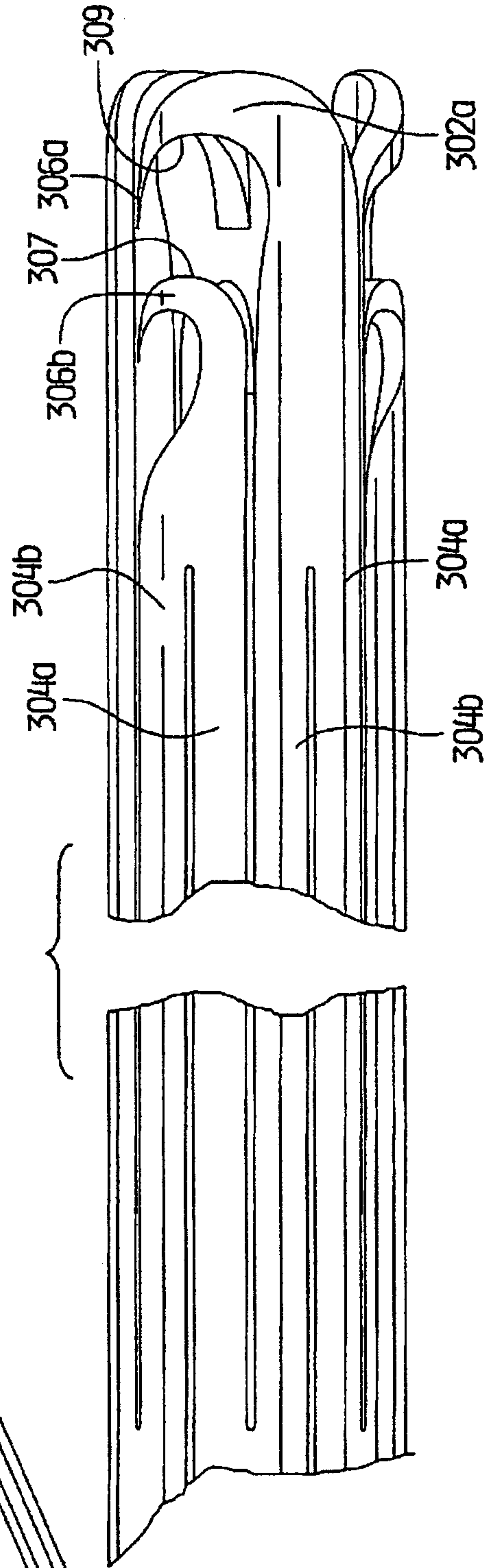


FIG. III



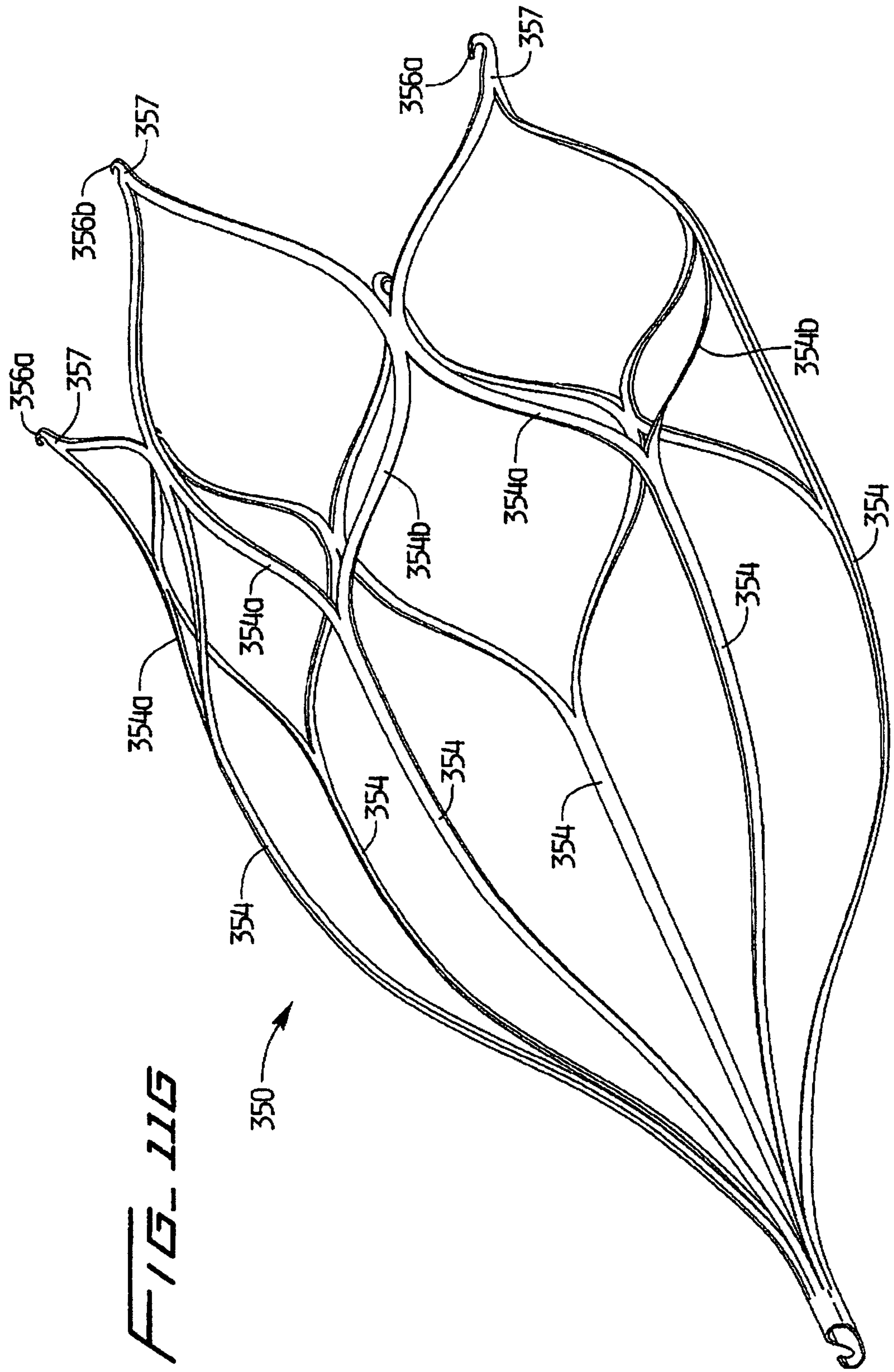


FIG. 11G

FIG. 11H

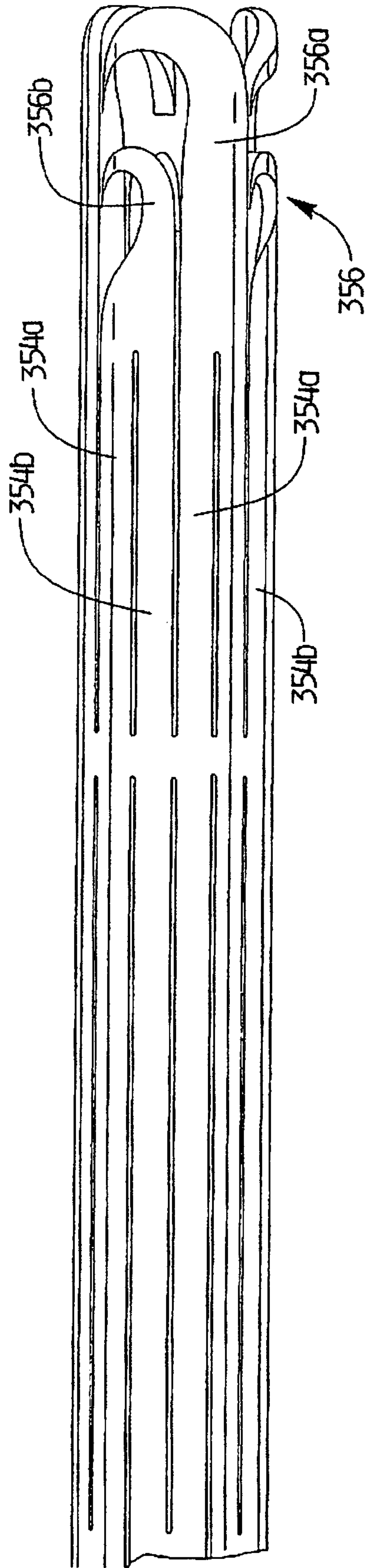


FIG. 12A

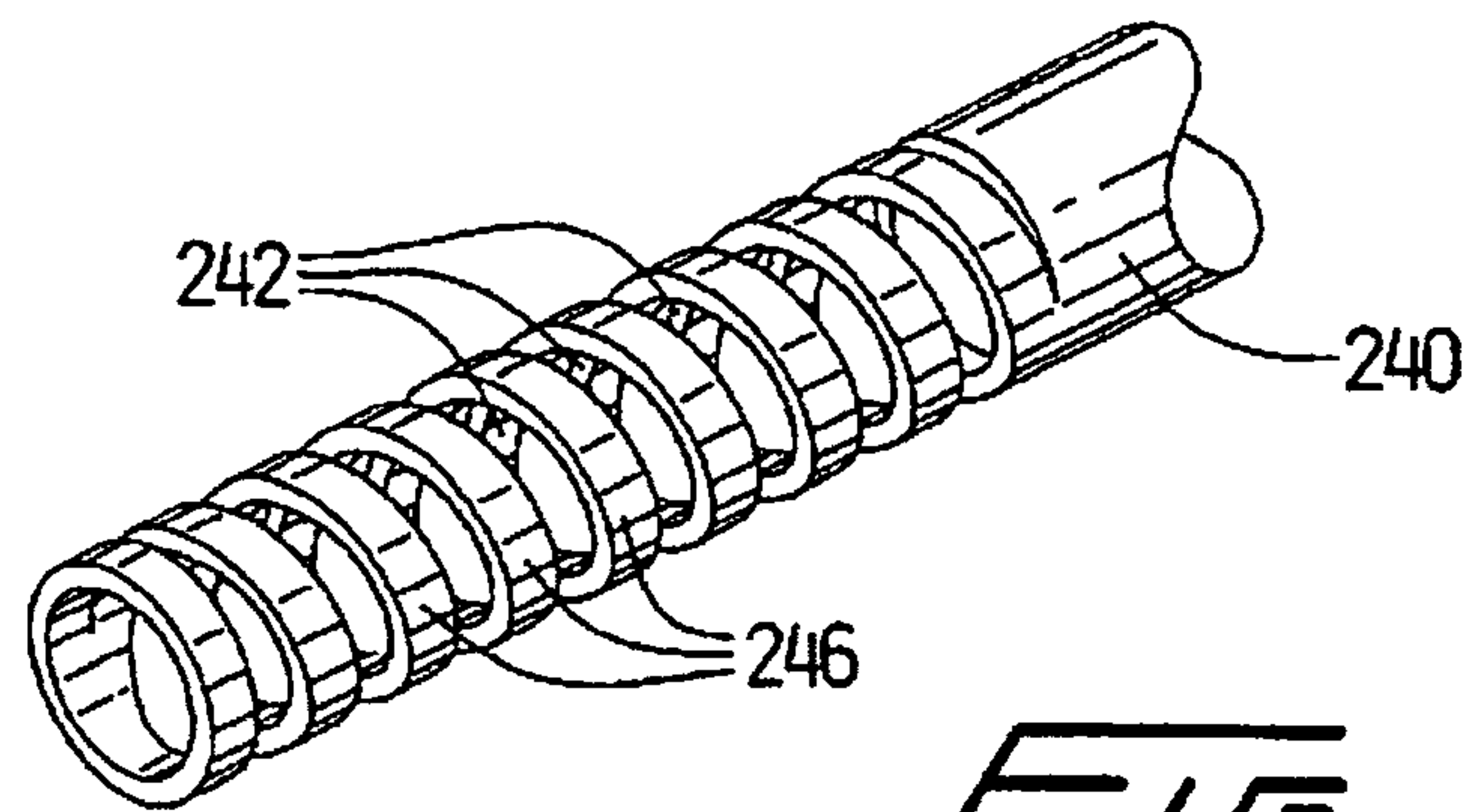
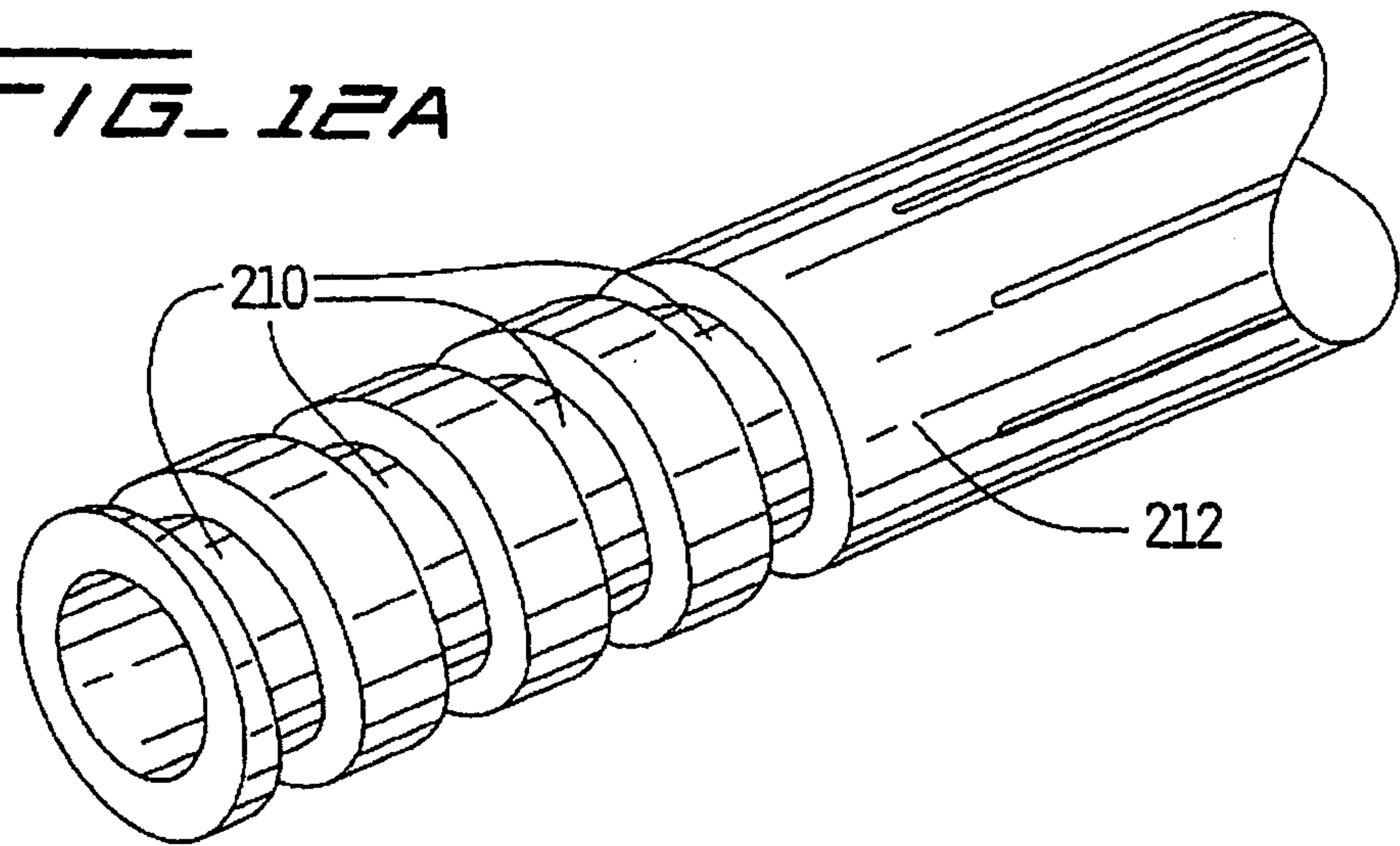


FIG. 12B

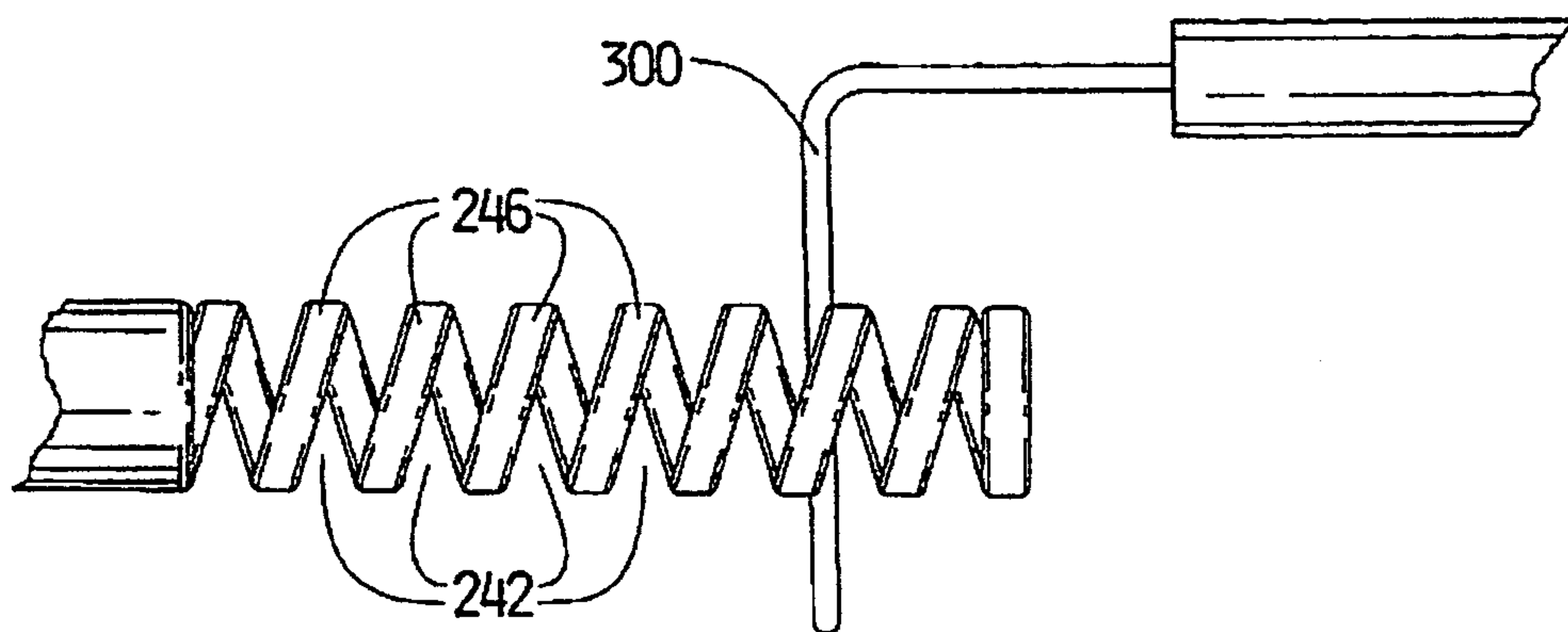


FIG. 12C

FIG. 13A

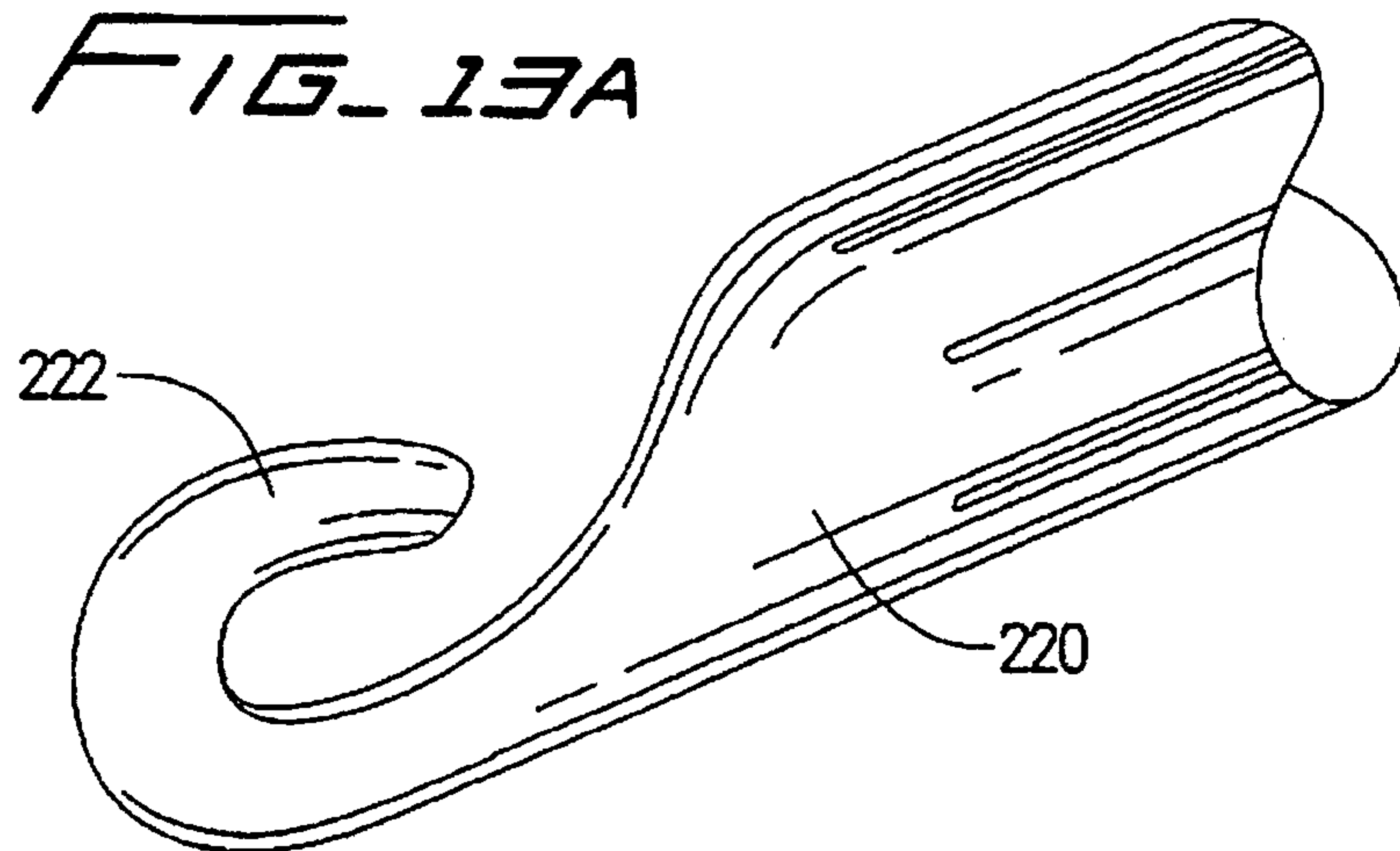


FIG. 13B

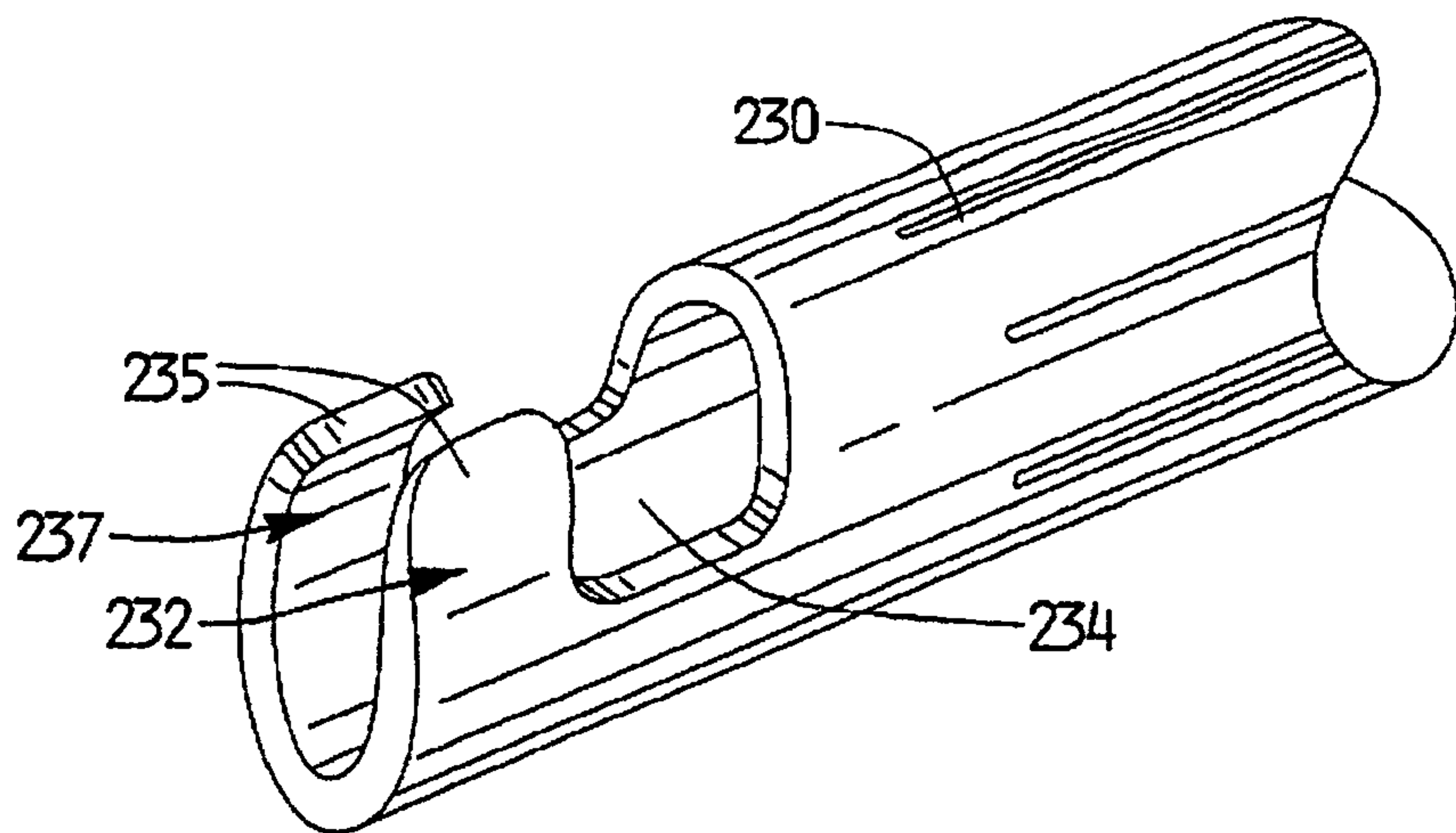


FIG. 13C

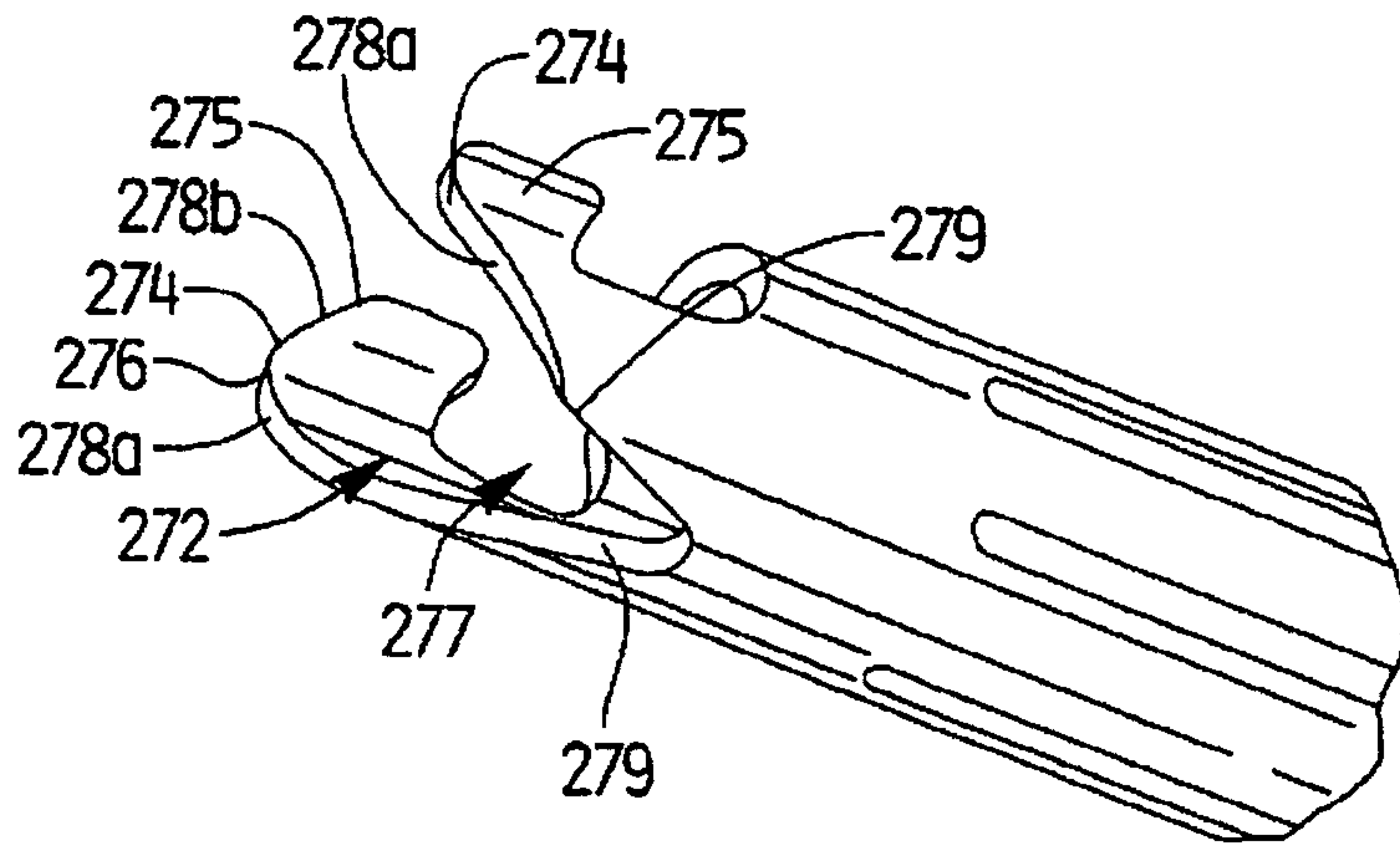


FIG. 13D

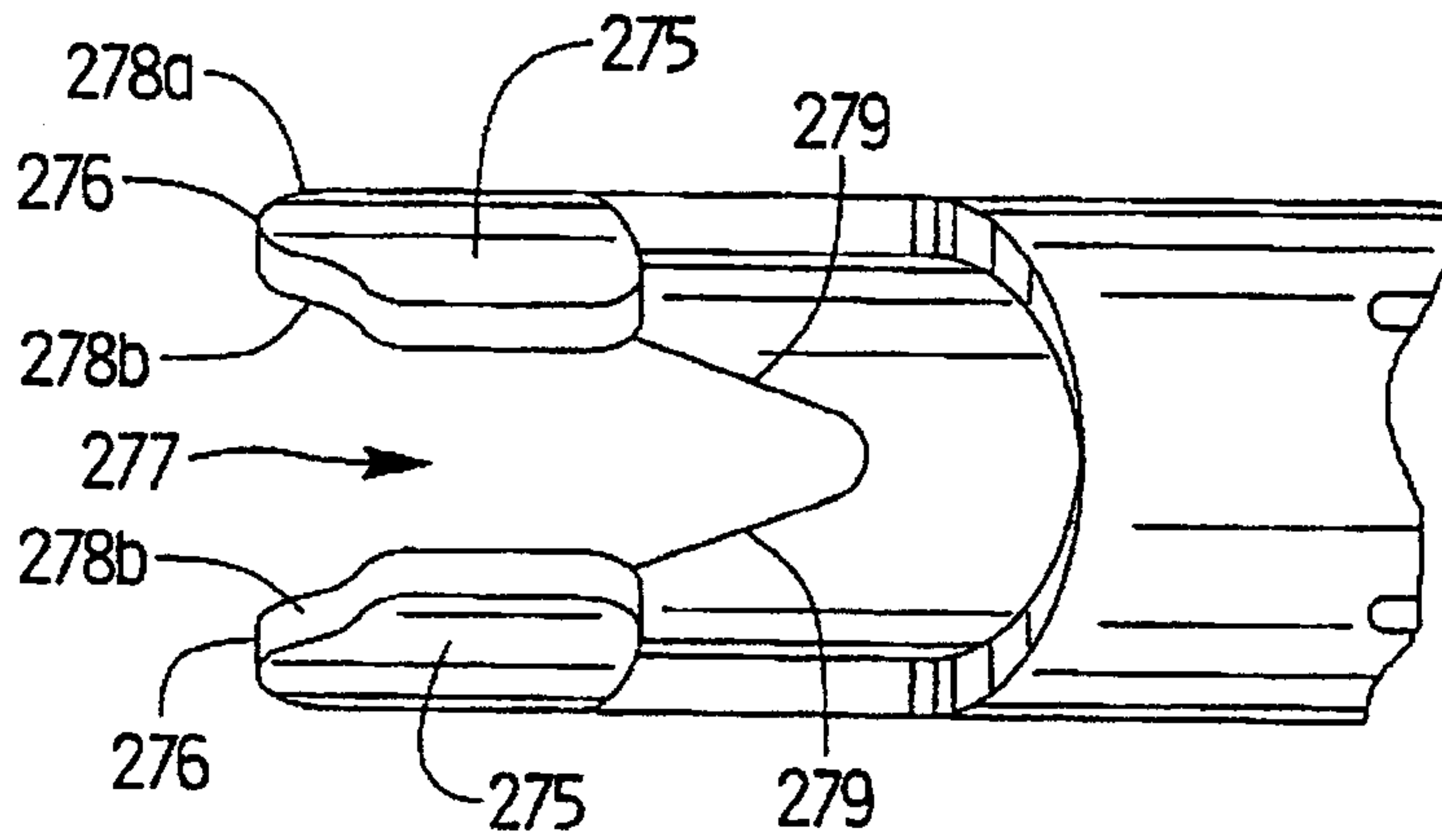


FIG. 13E

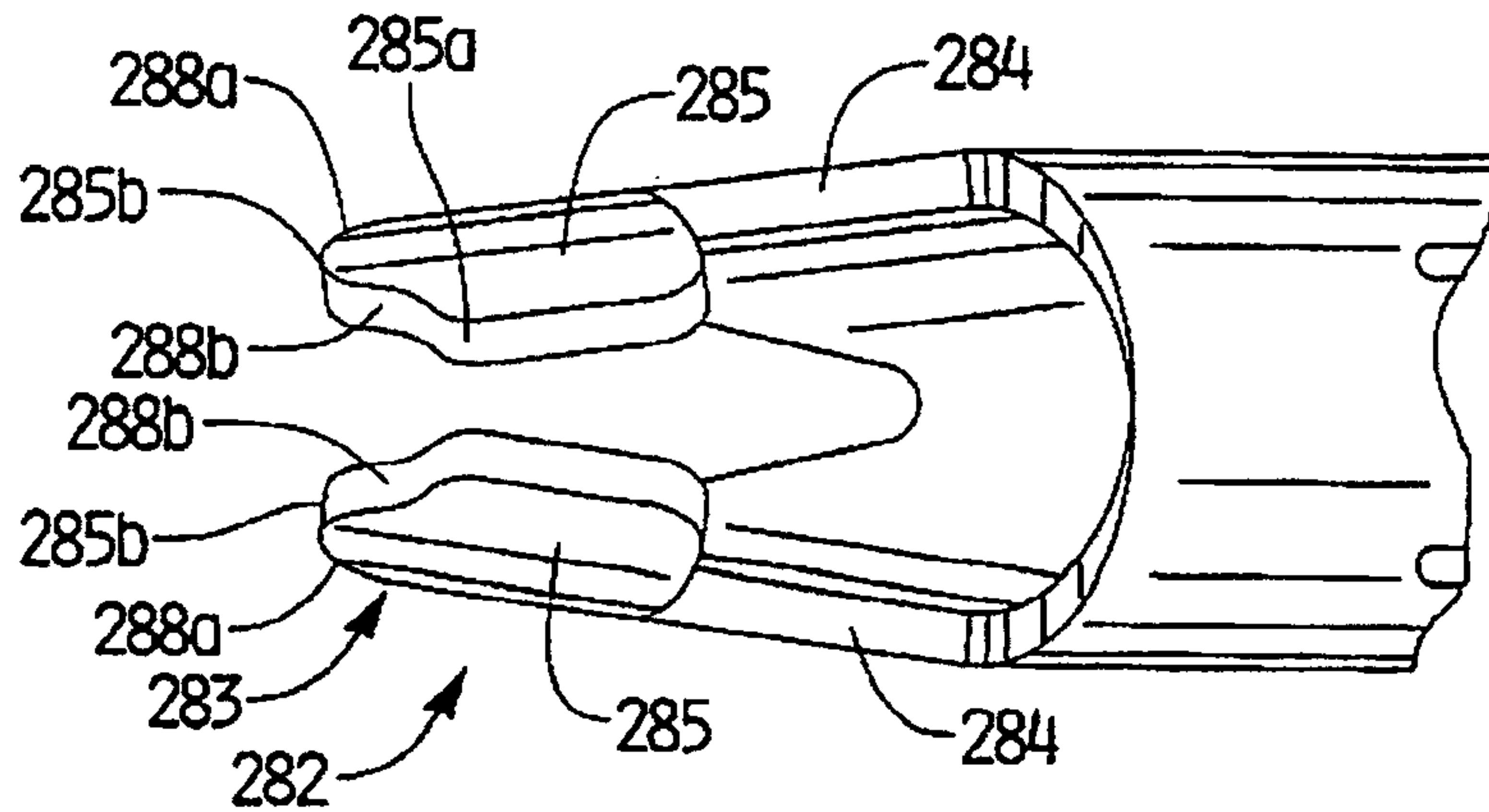


FIG. 13F

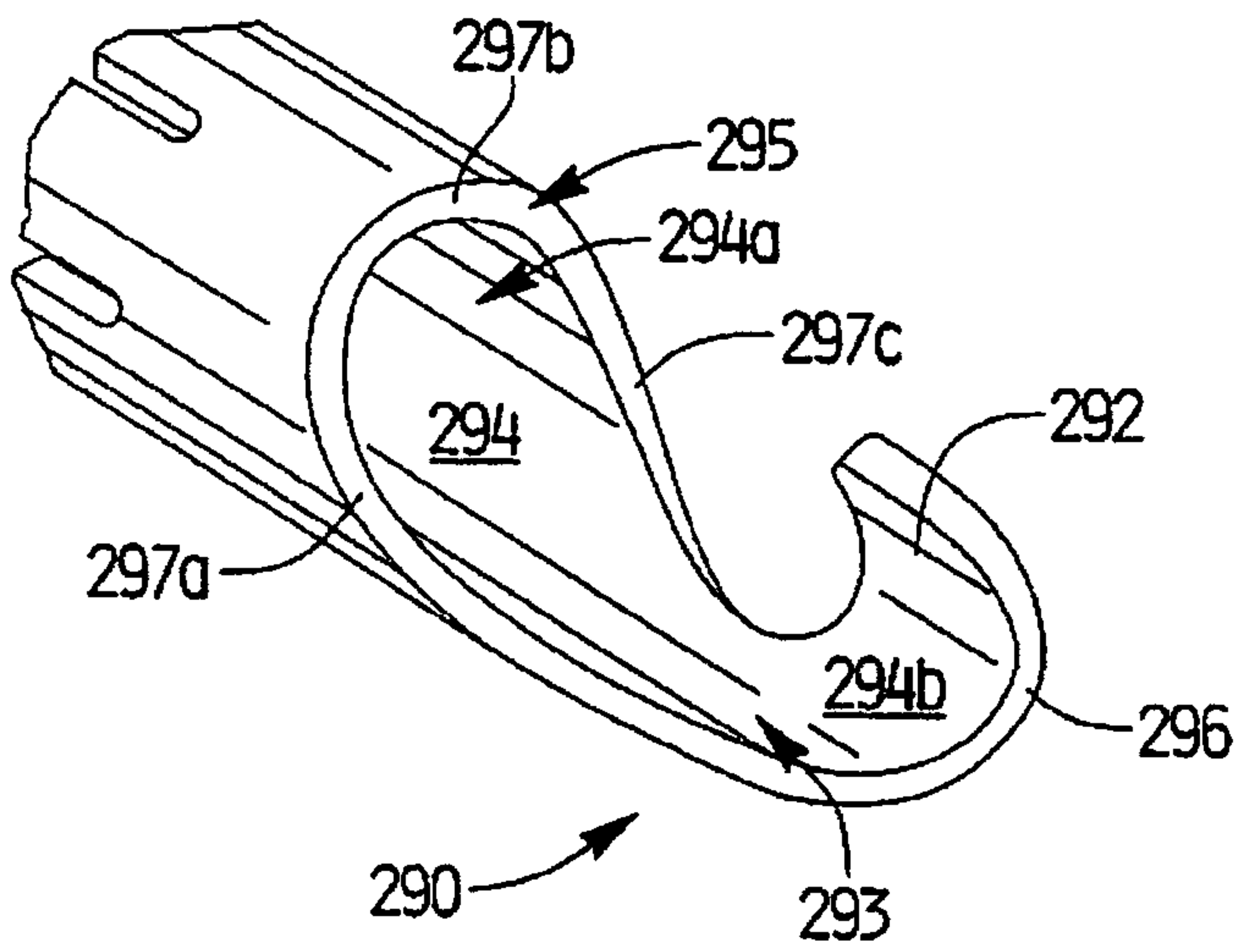


FIG. 13G

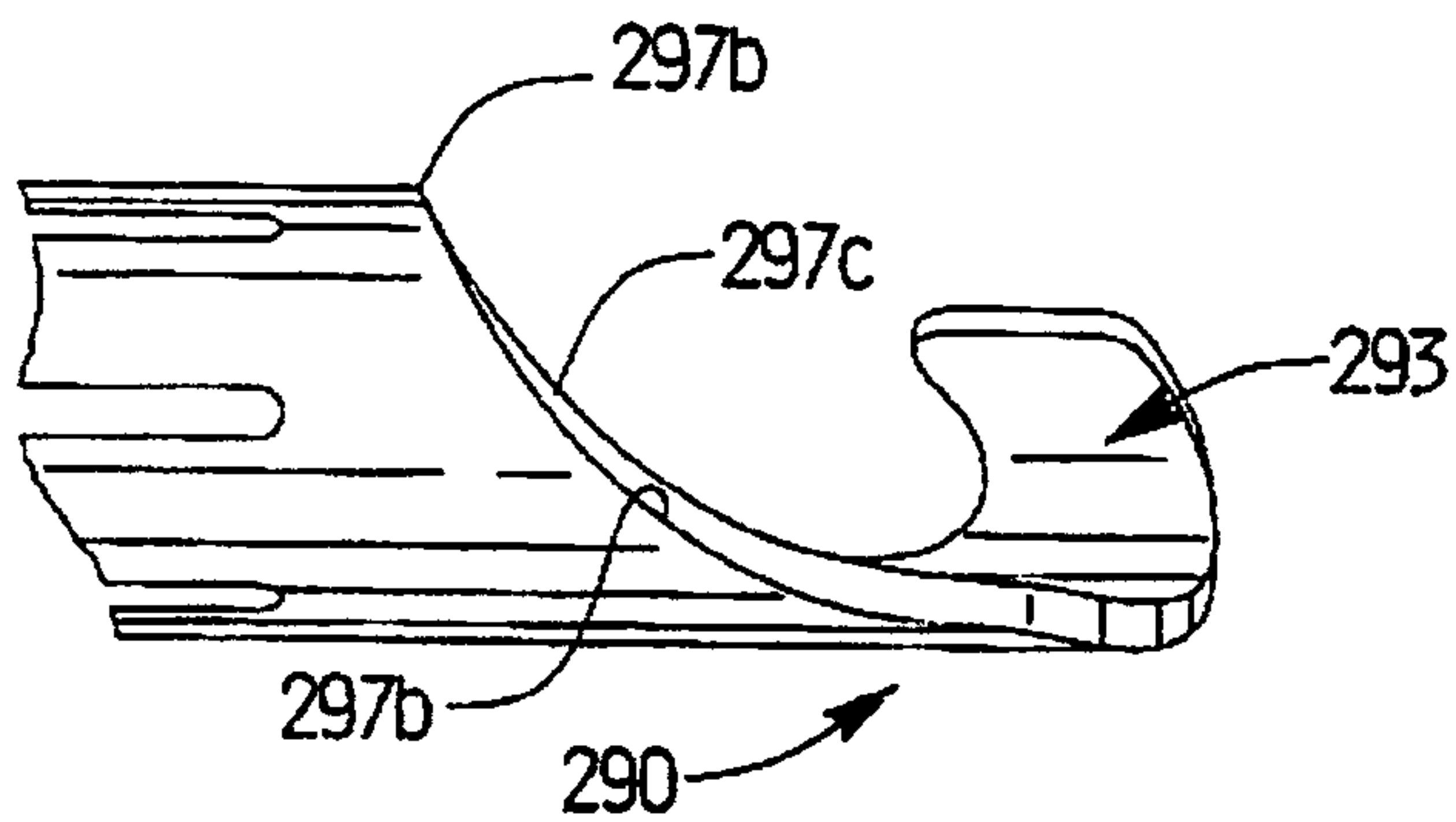


FIG. 13H

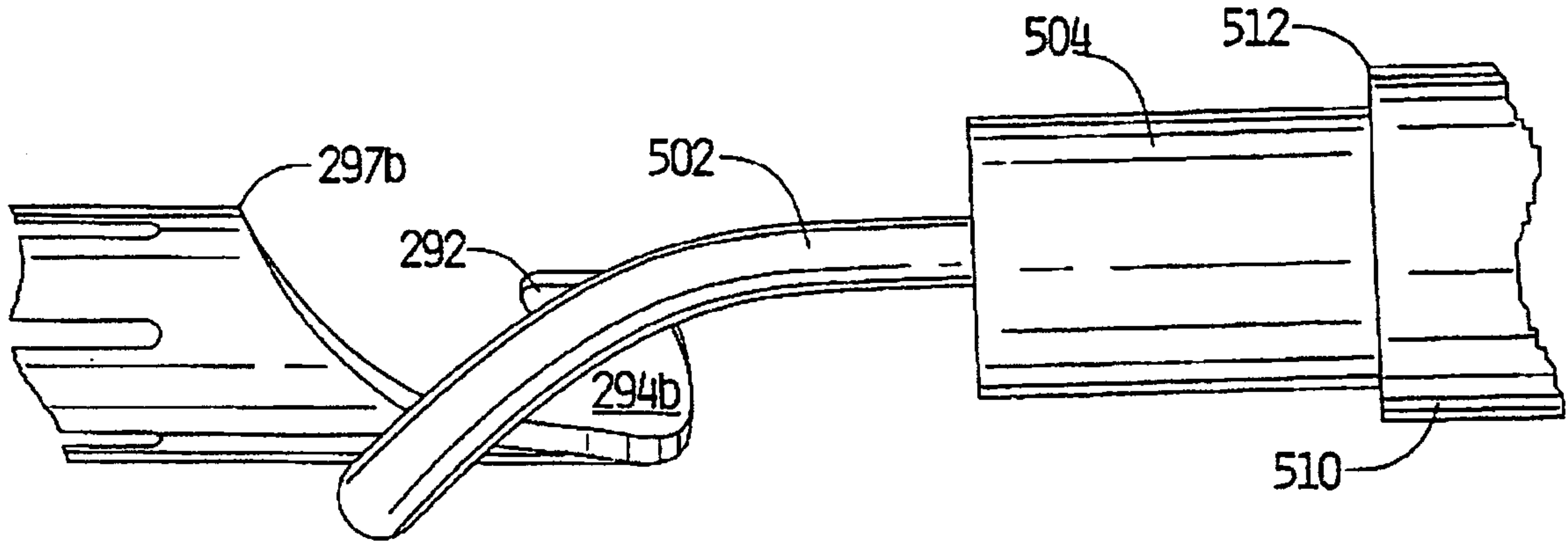


FIG. 13I

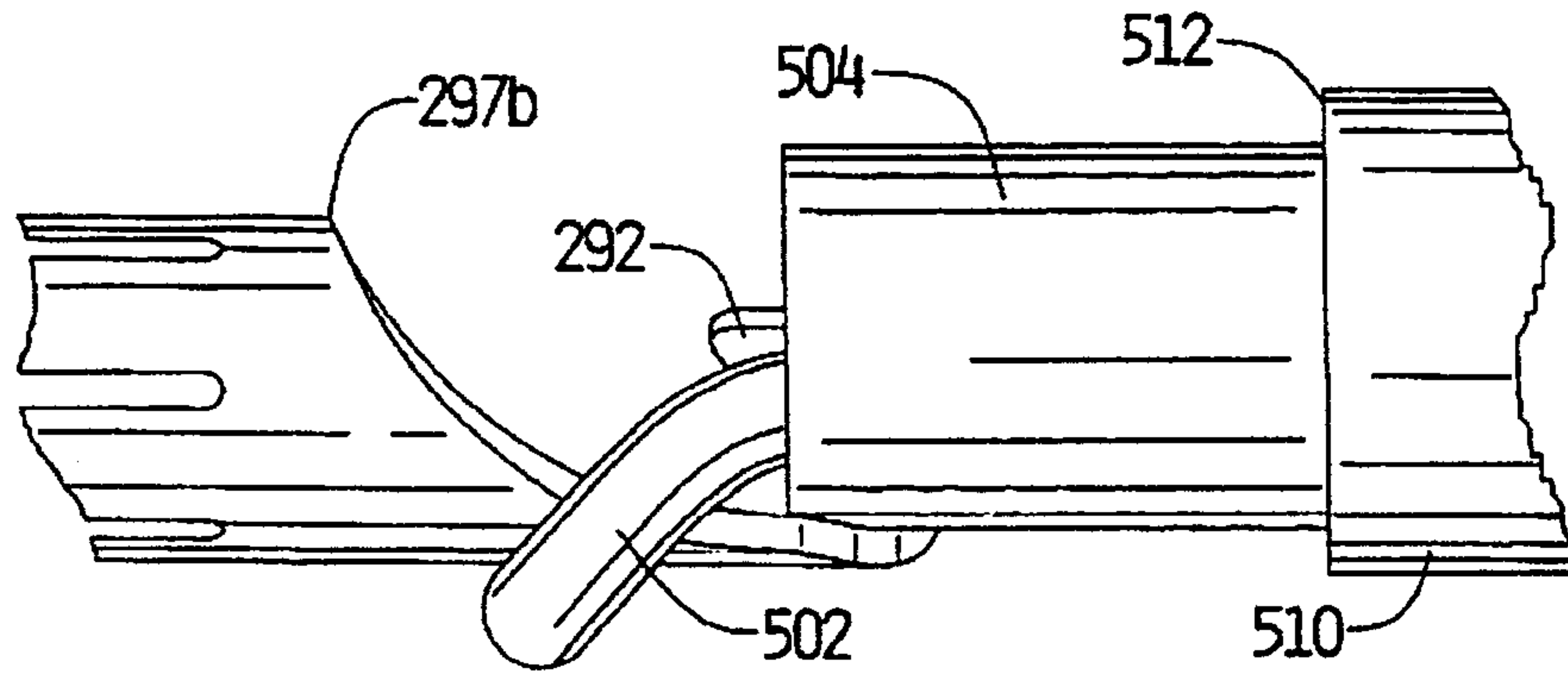
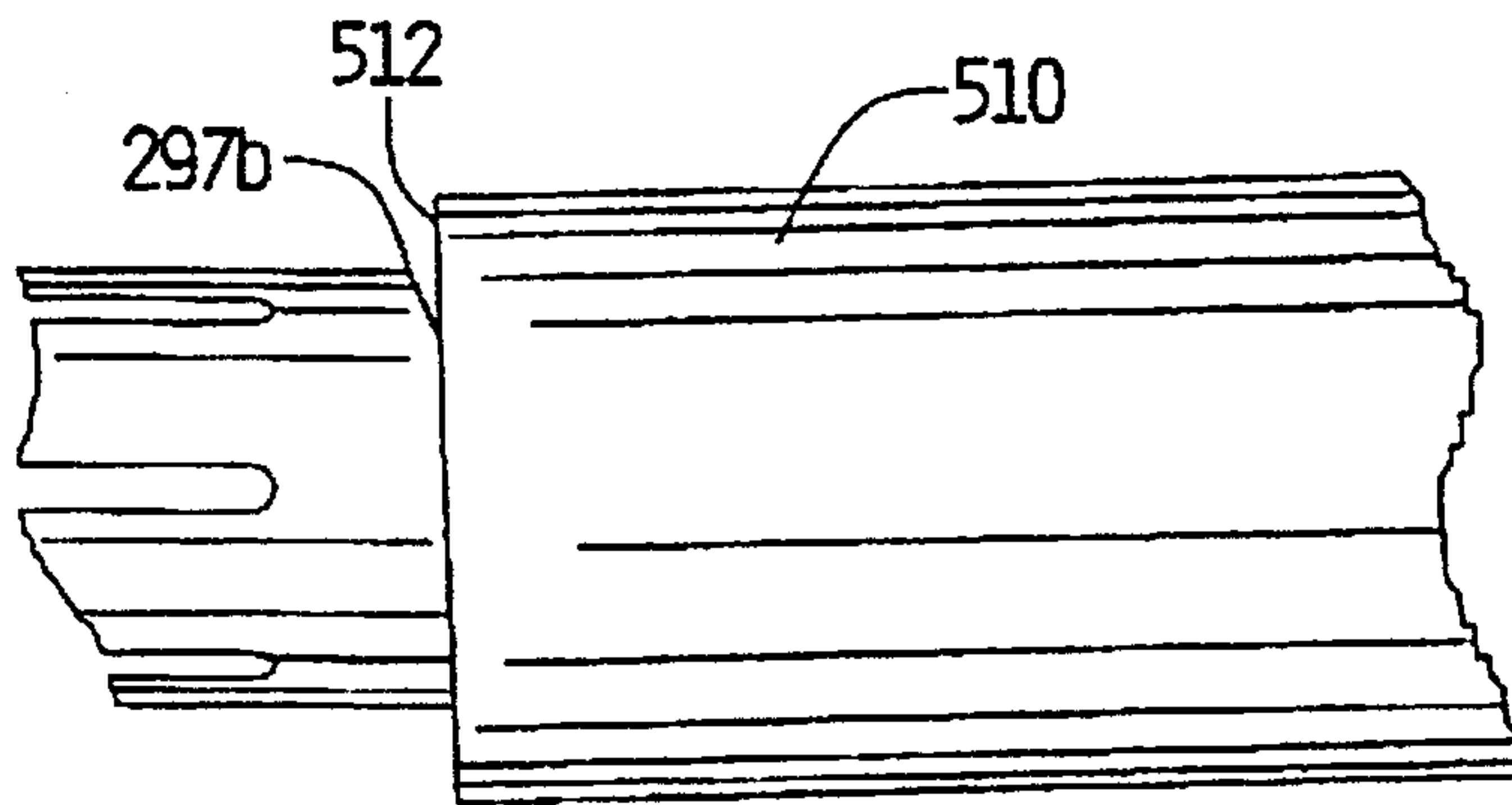


FIG. 13J



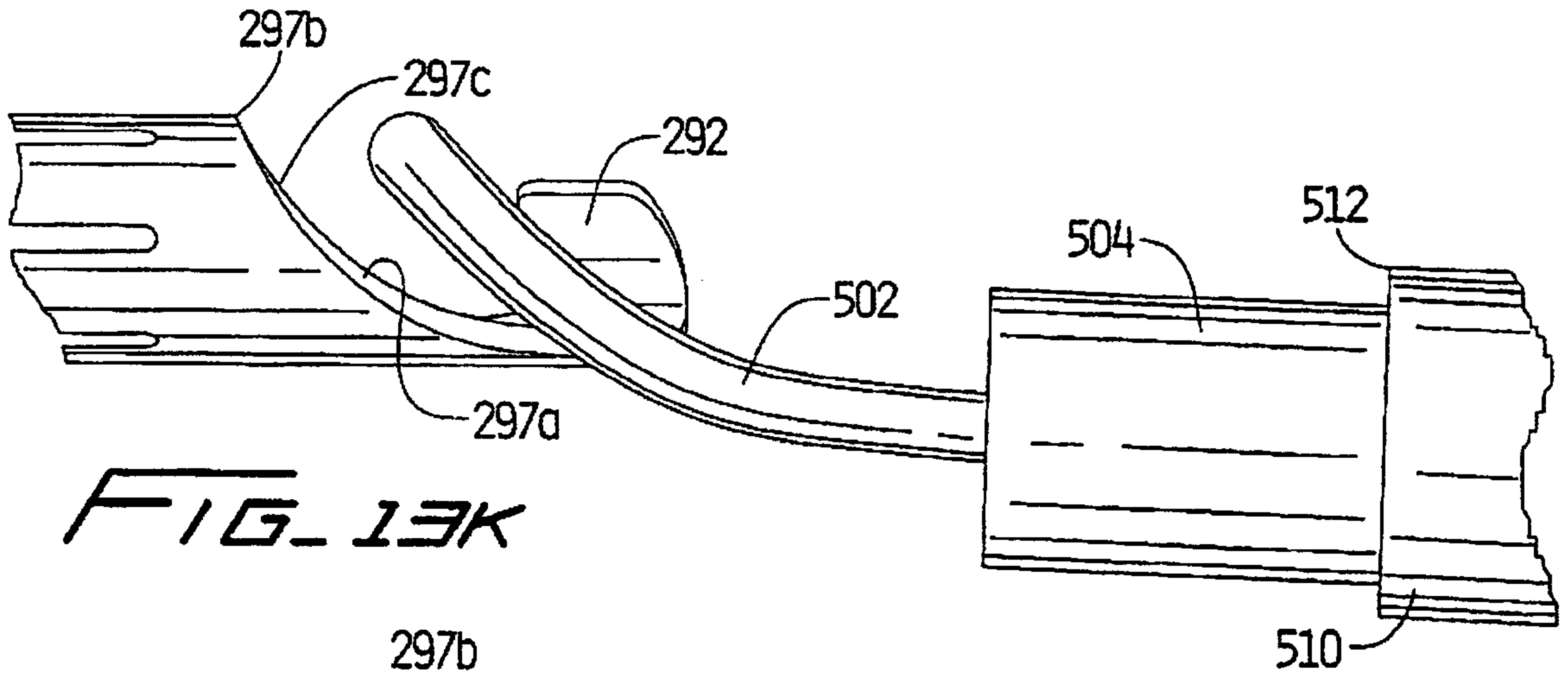


FIG. 13K

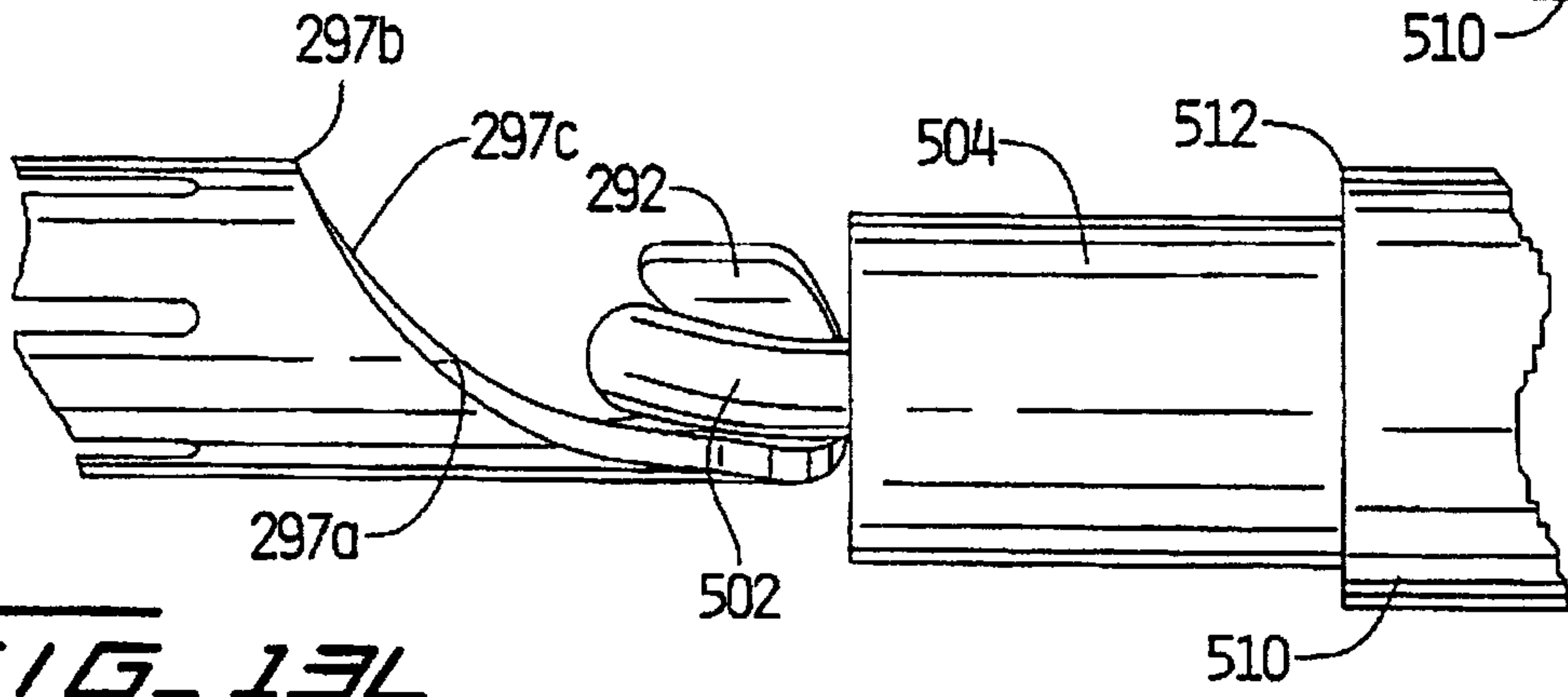


FIG. 13L

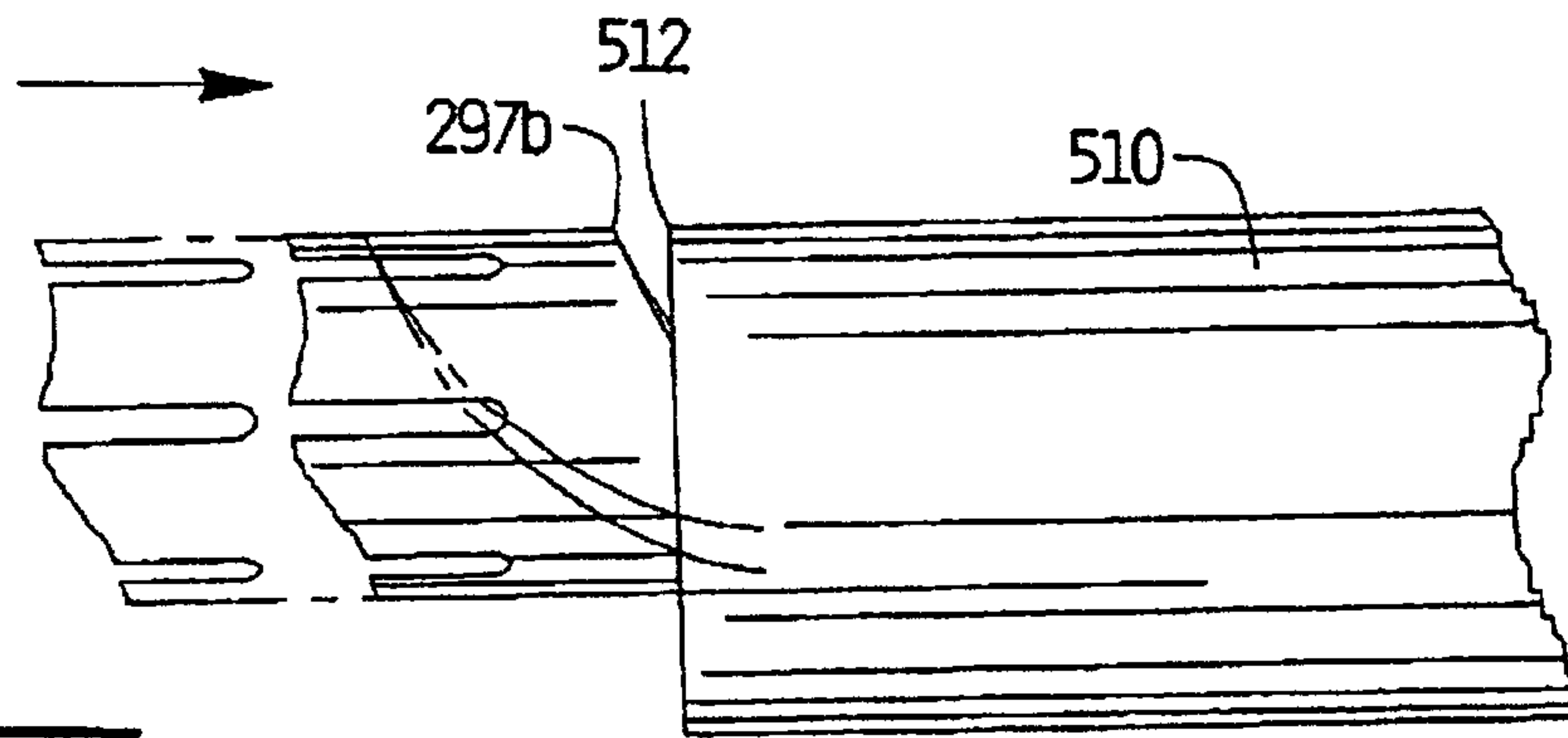


FIG. 13M

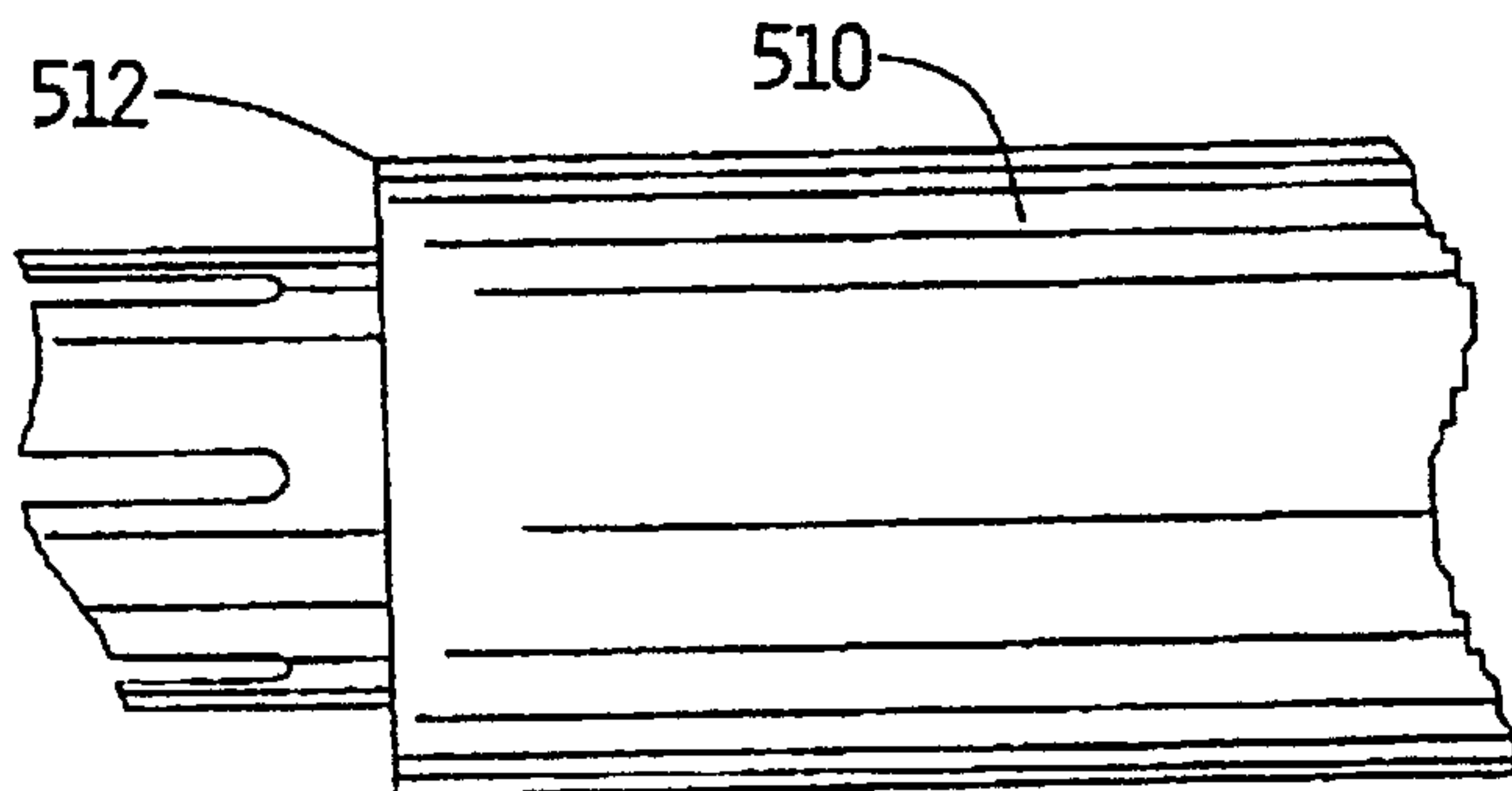


FIG. 13N

FIG. 14

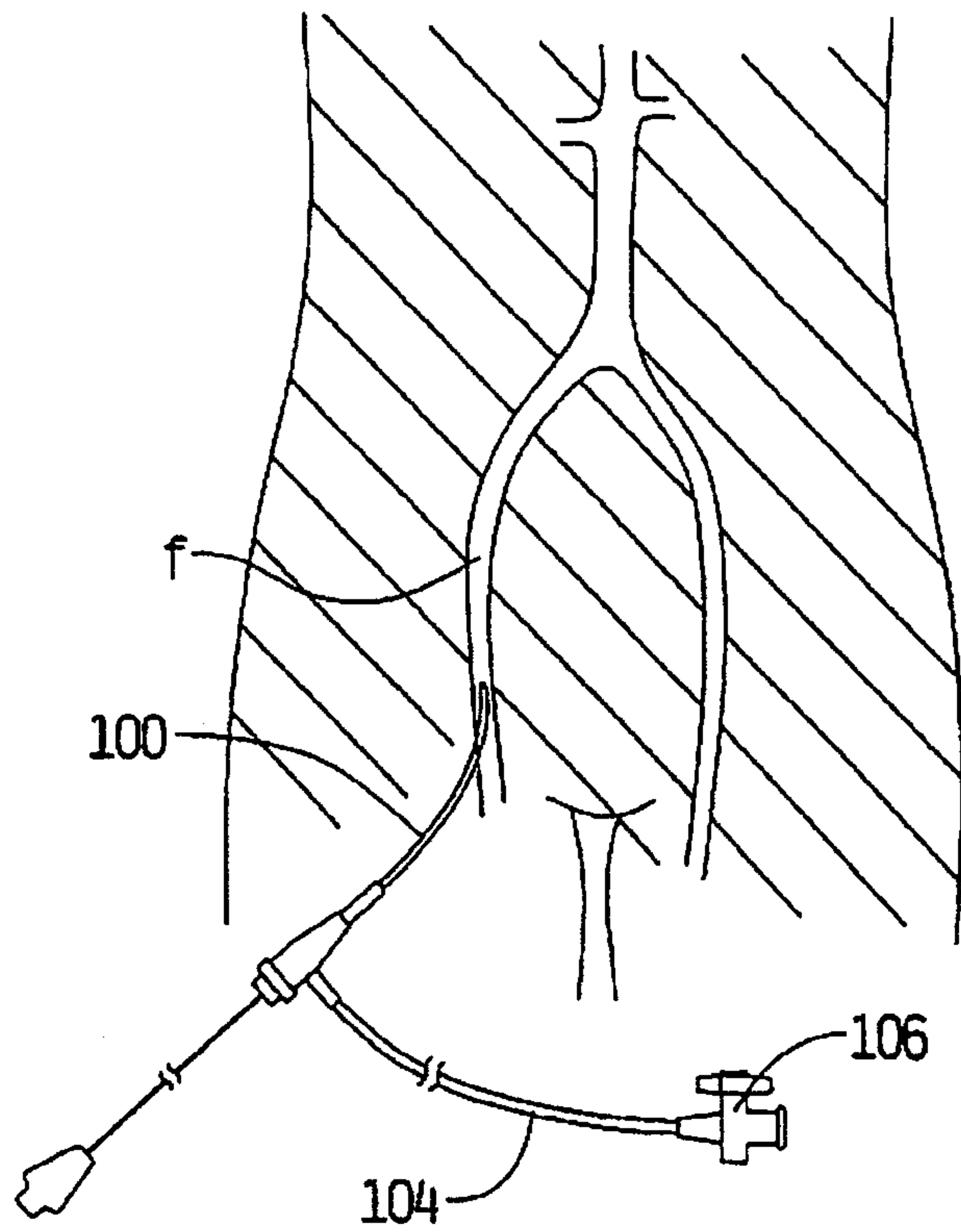


FIG. 15

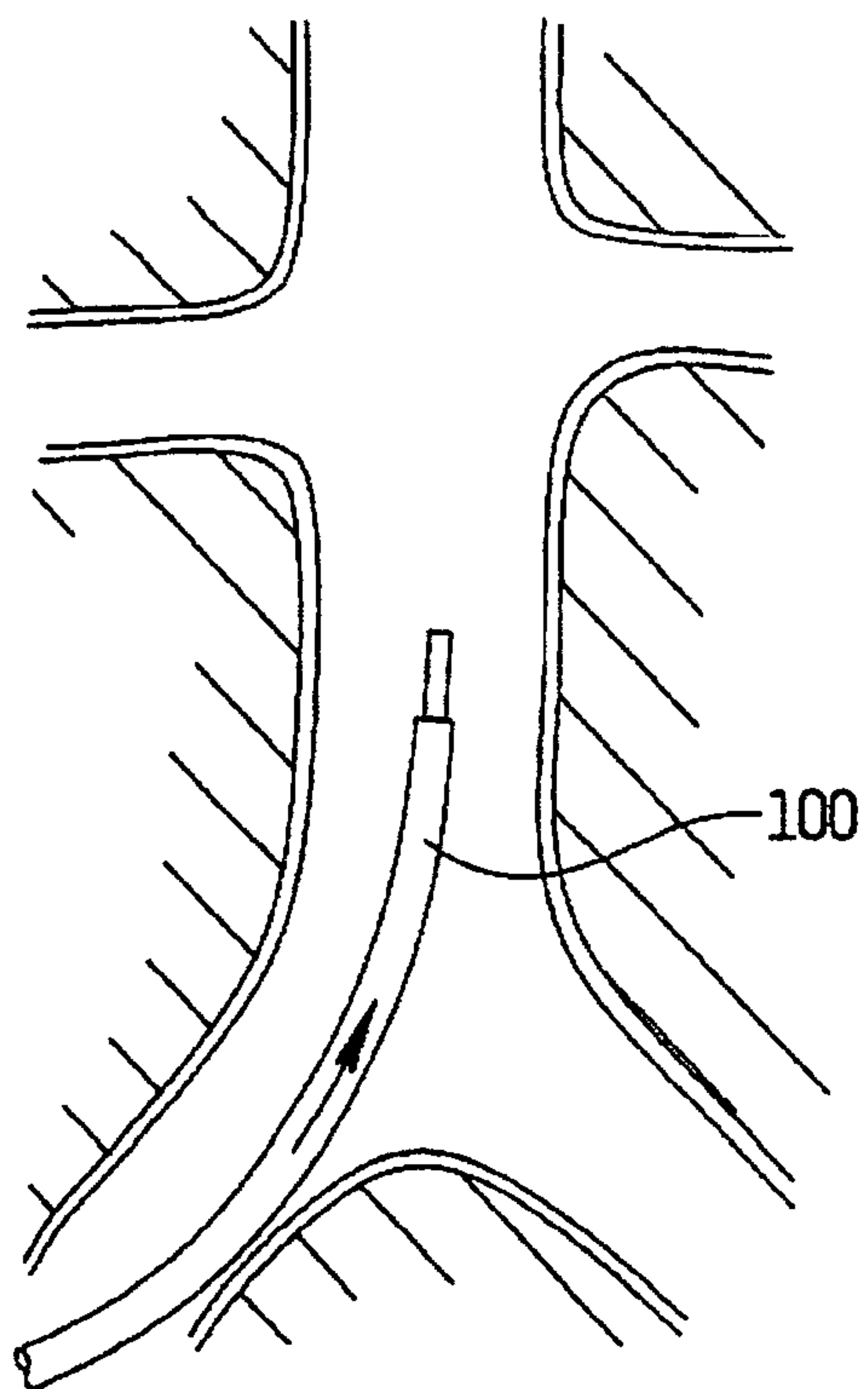
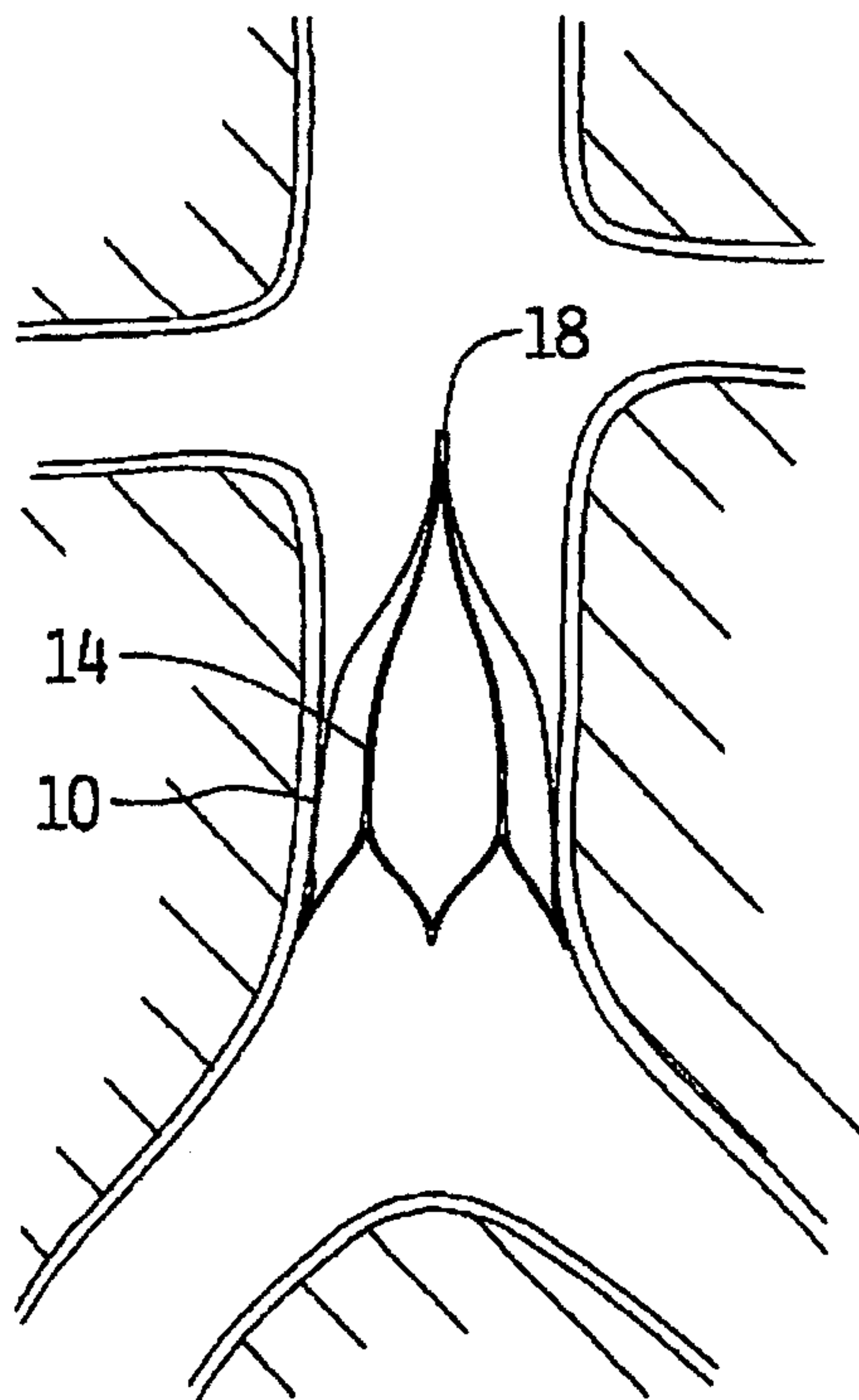


FIG. 16



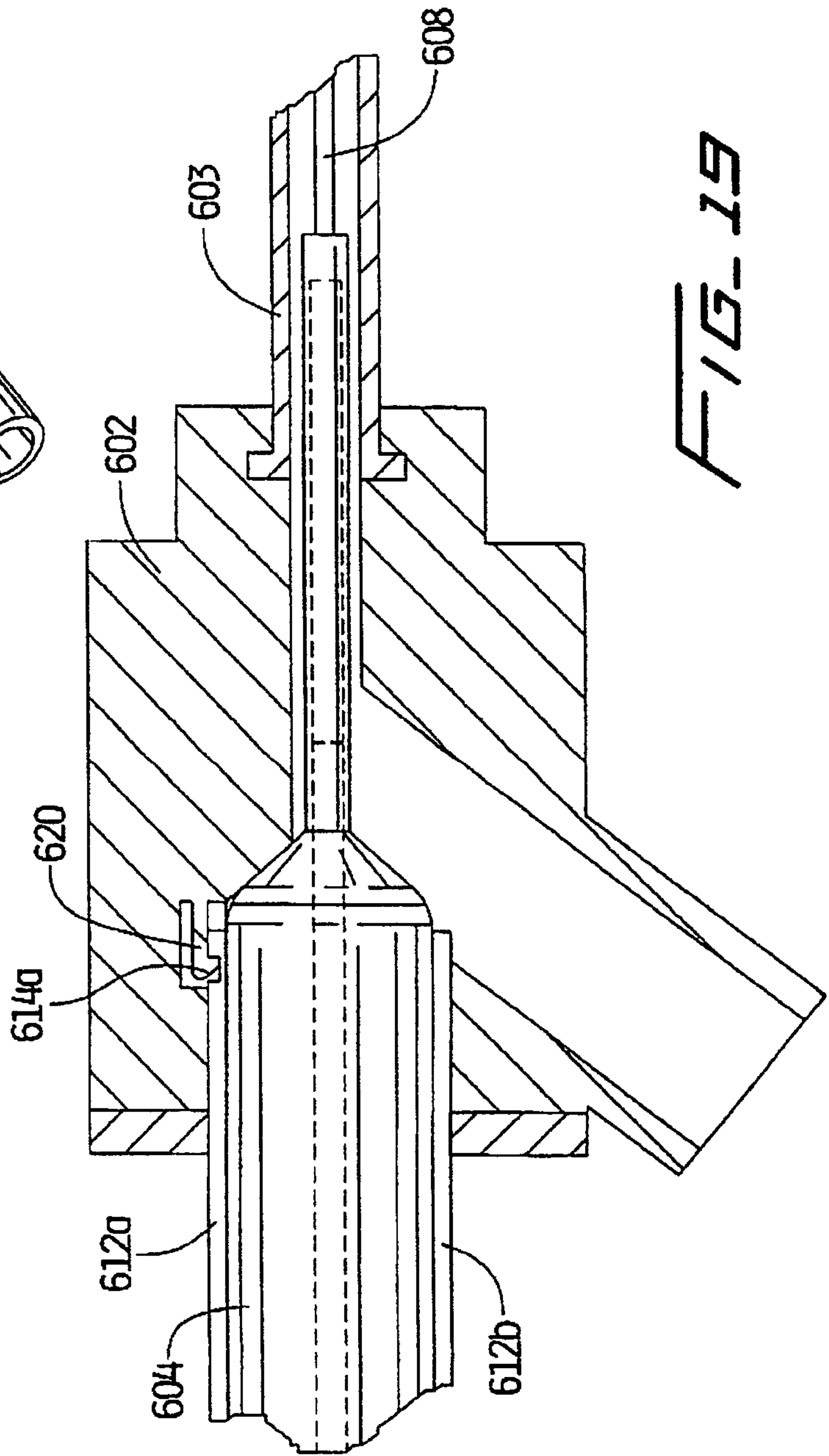
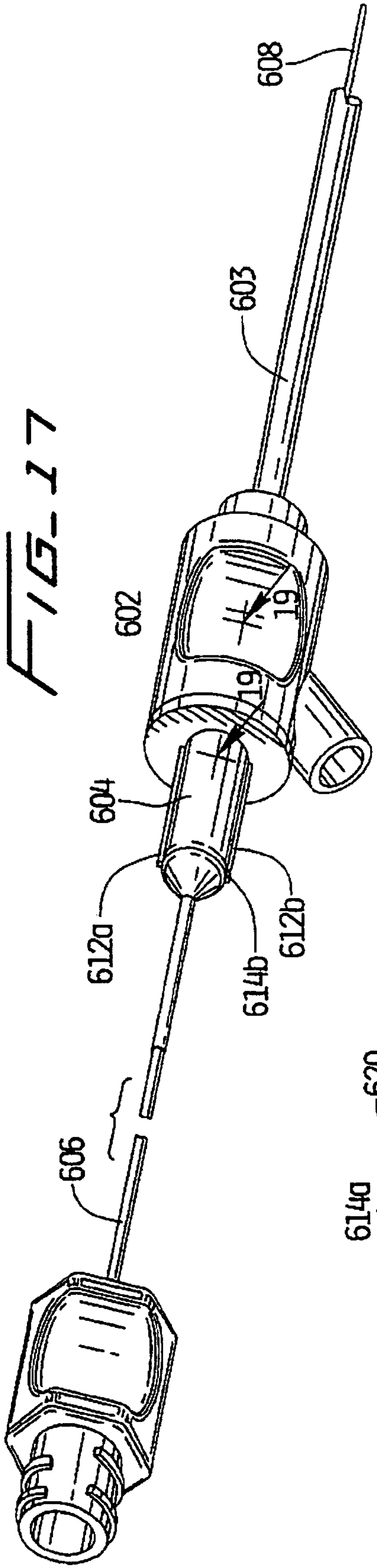
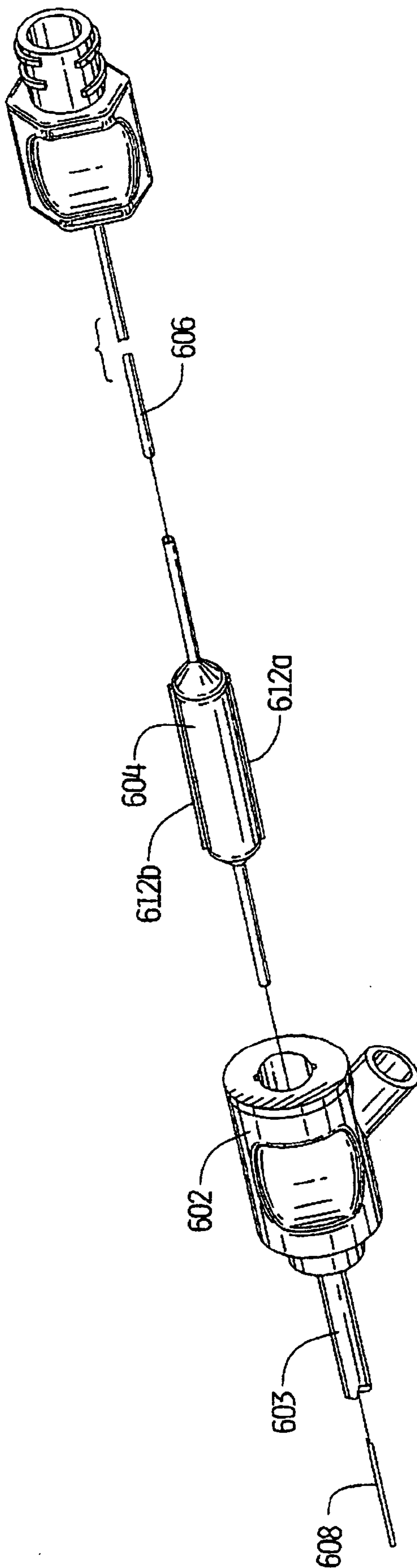


FIG. 1B



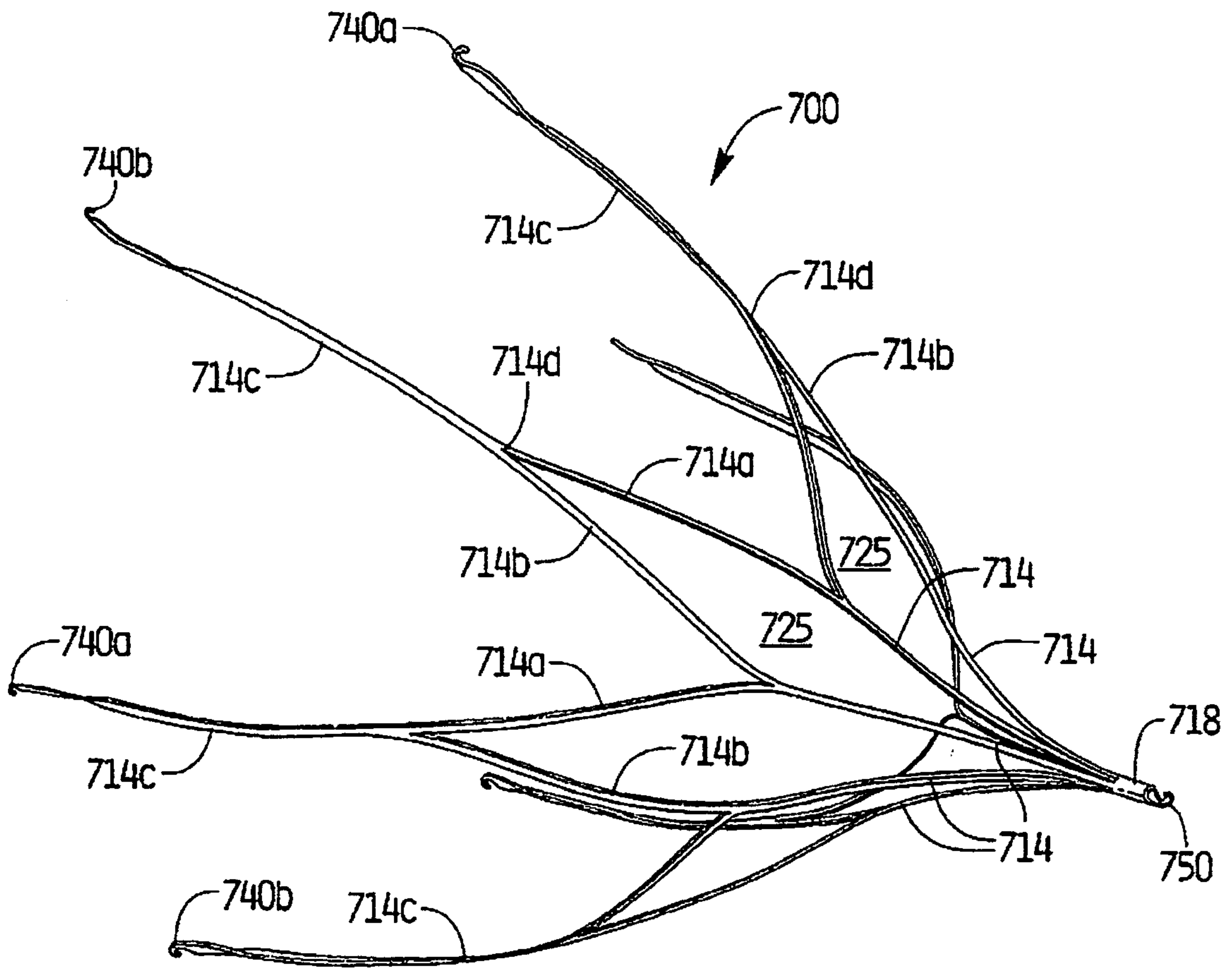


FIG. 20A

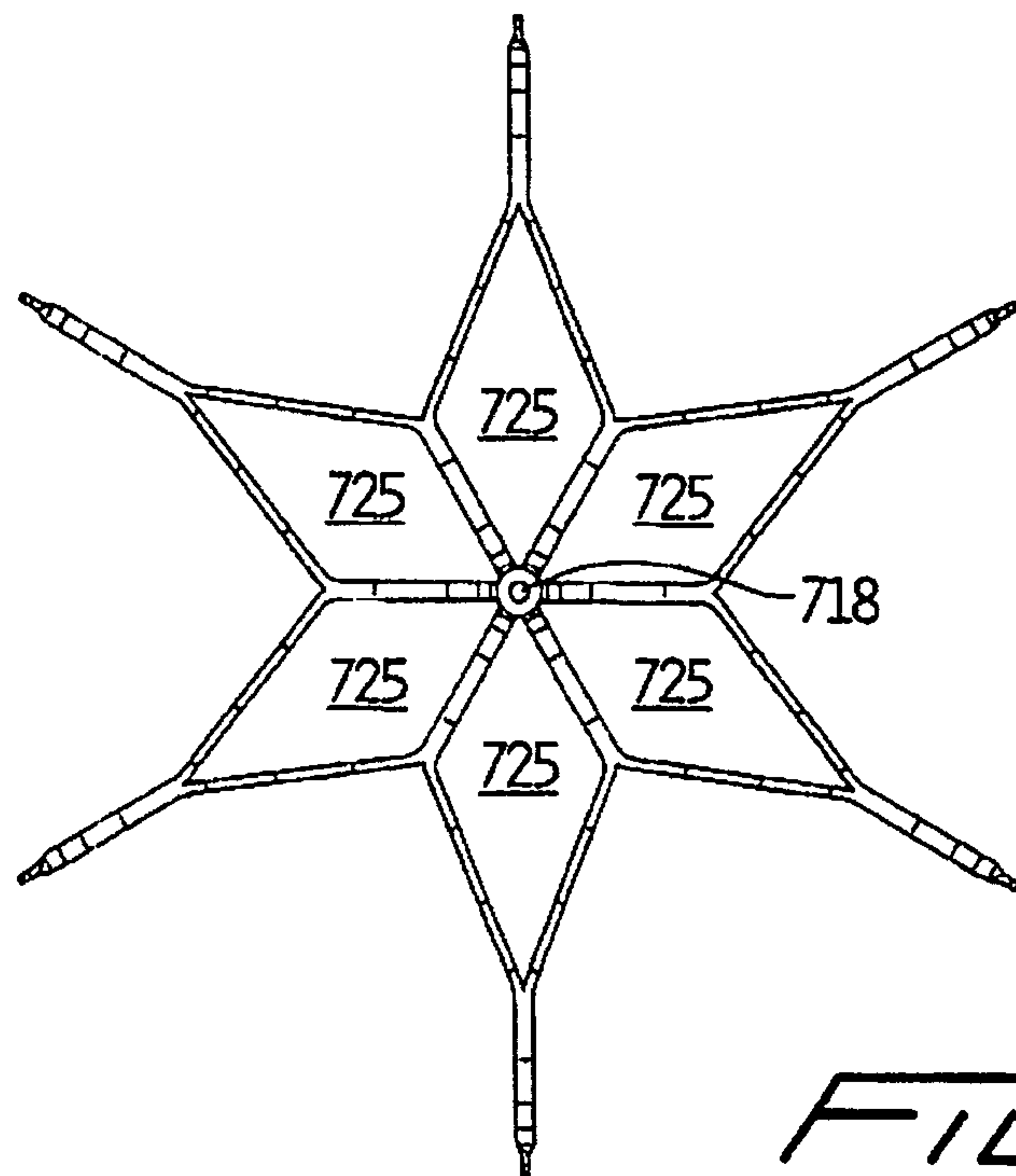


FIG. 20B

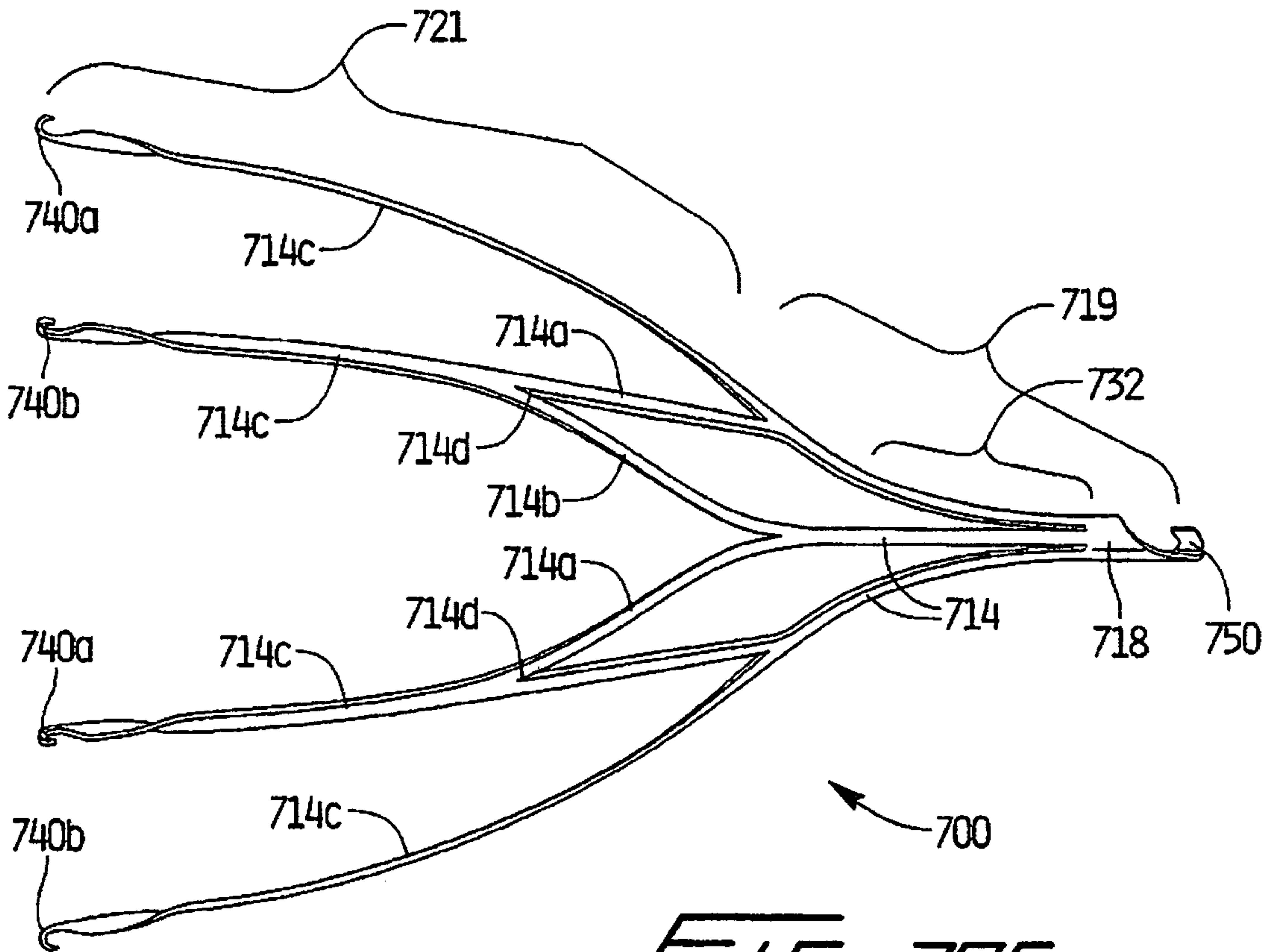


FIG. 20C

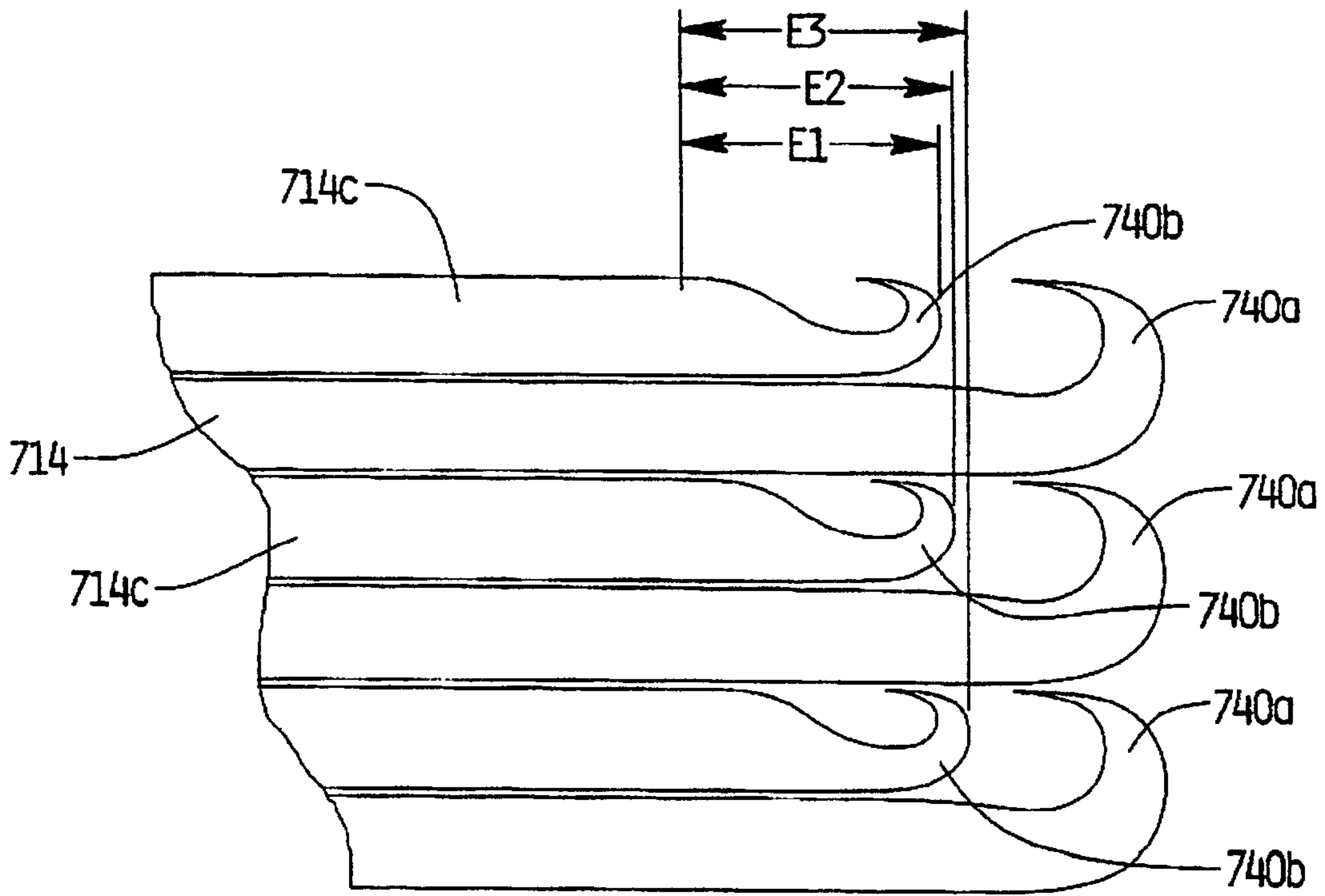


FIG. 20F

FIG. 200

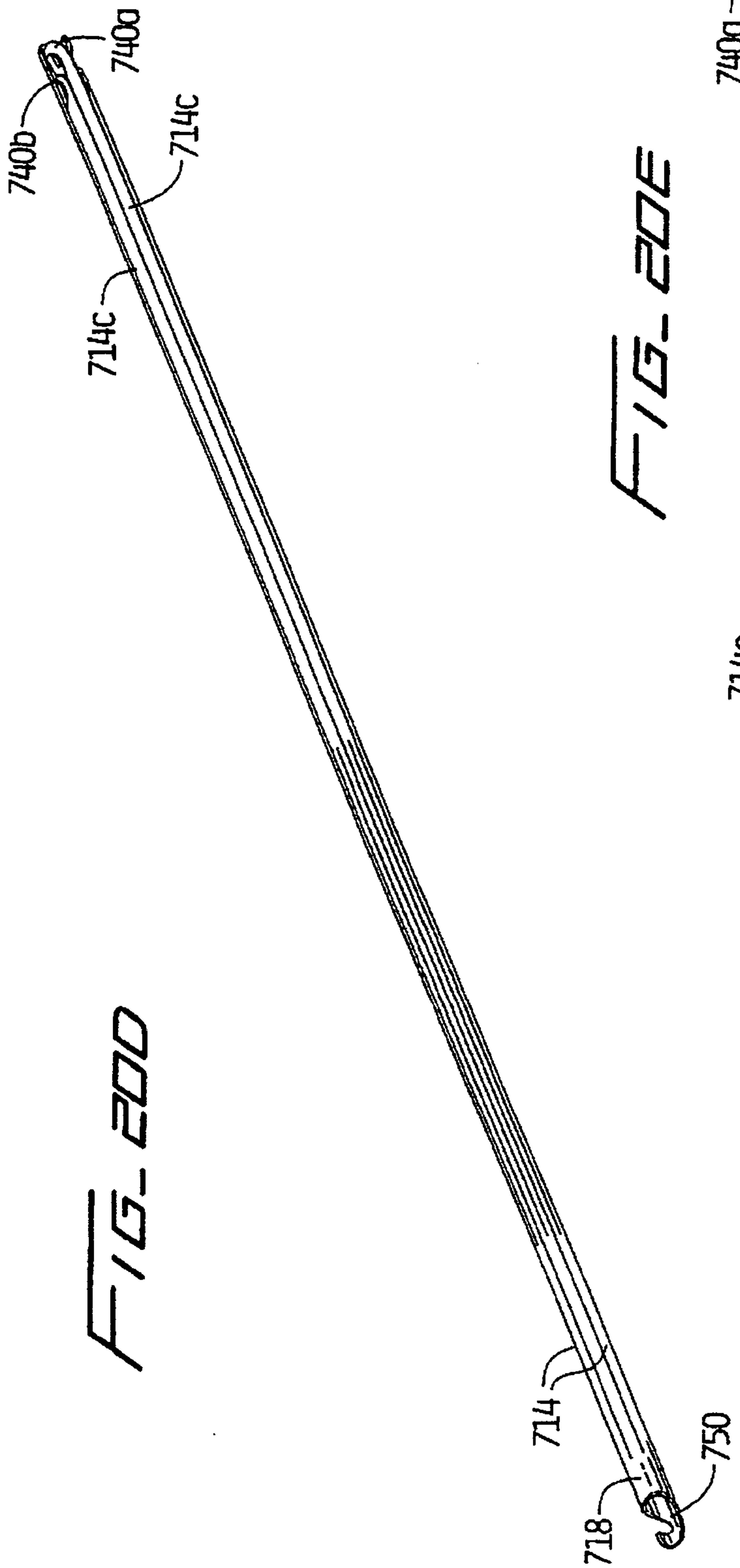


FIG. 200E

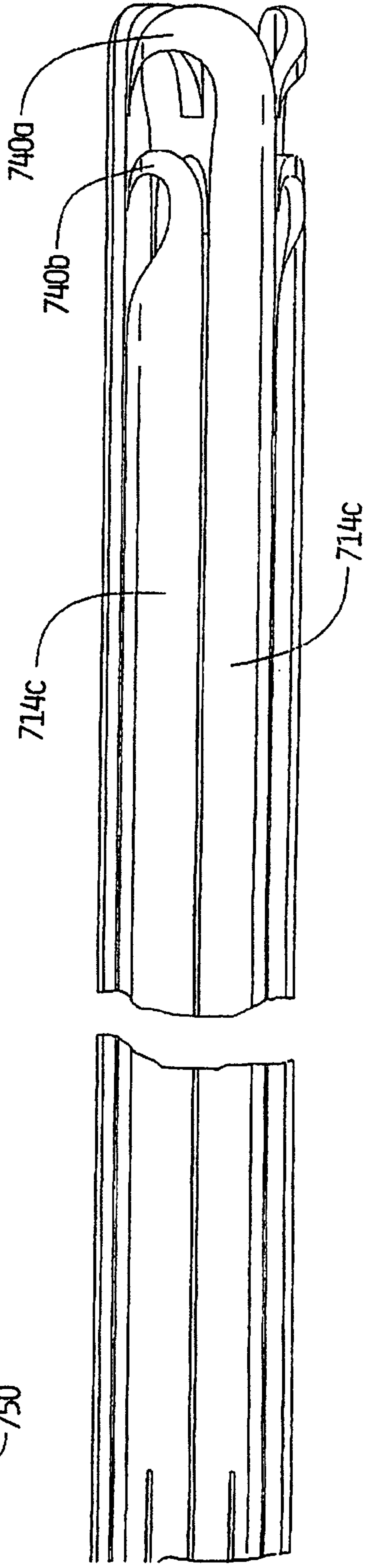


FIG. 21

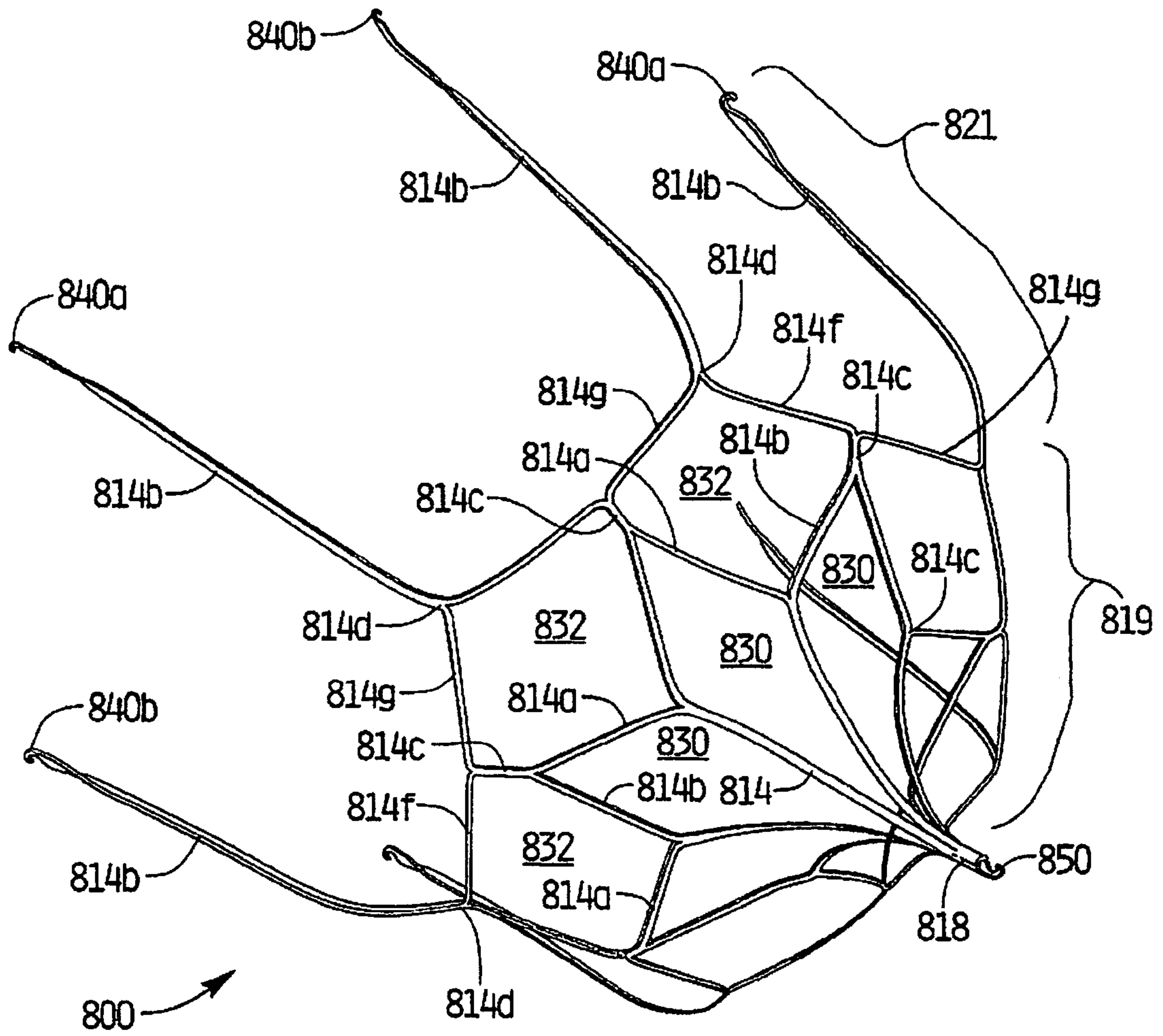


FIG. 22A

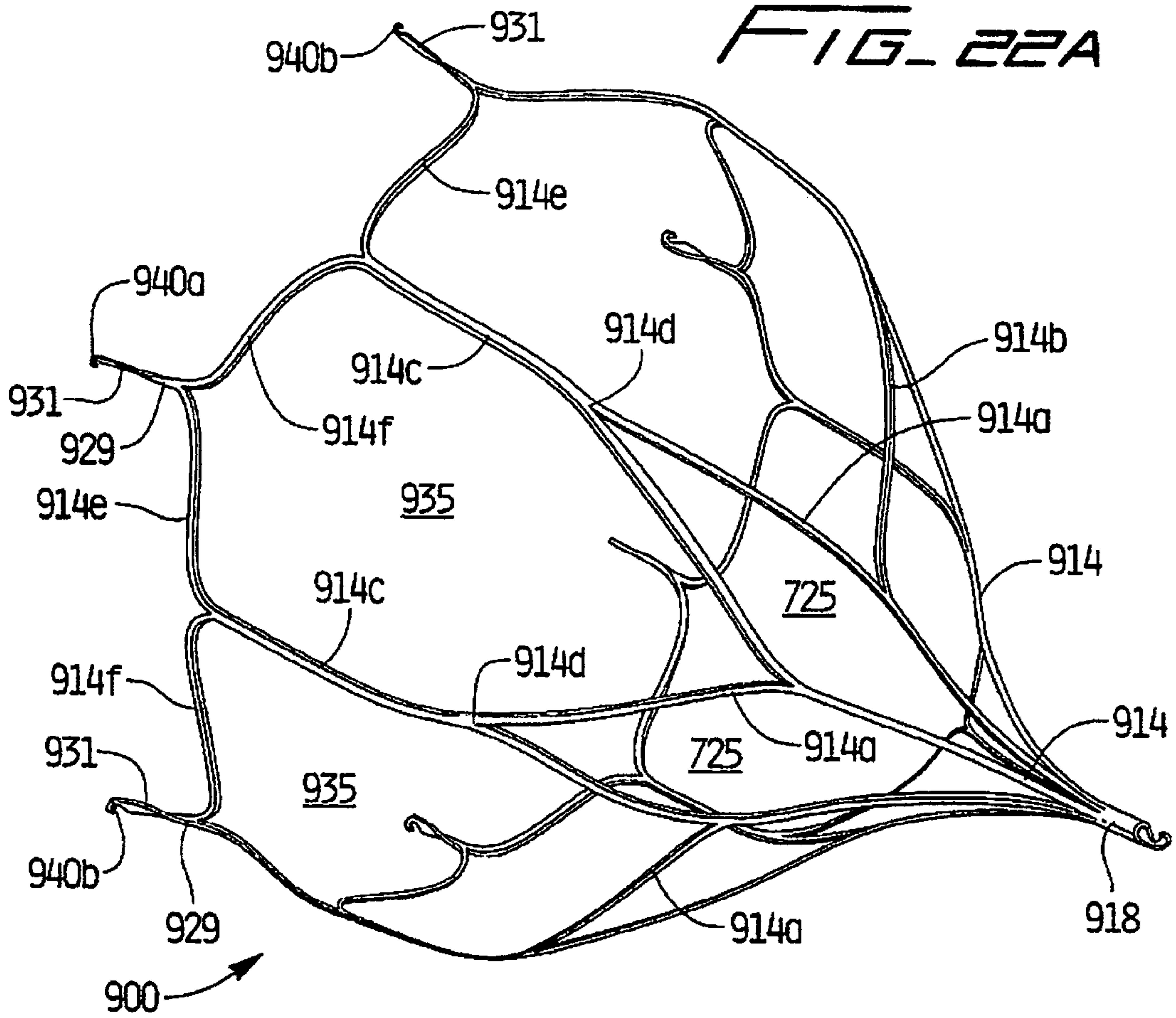
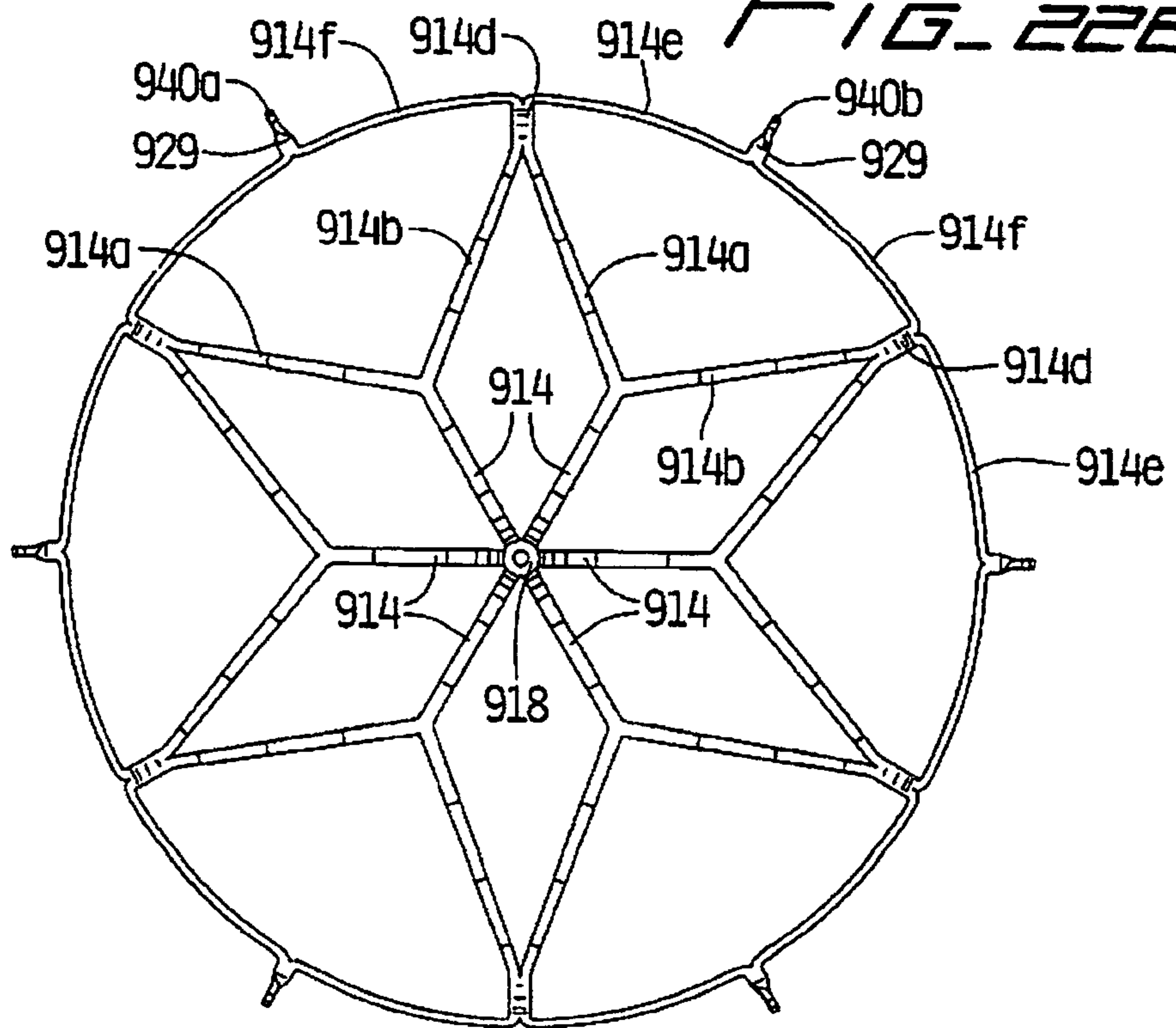


FIG. 22B



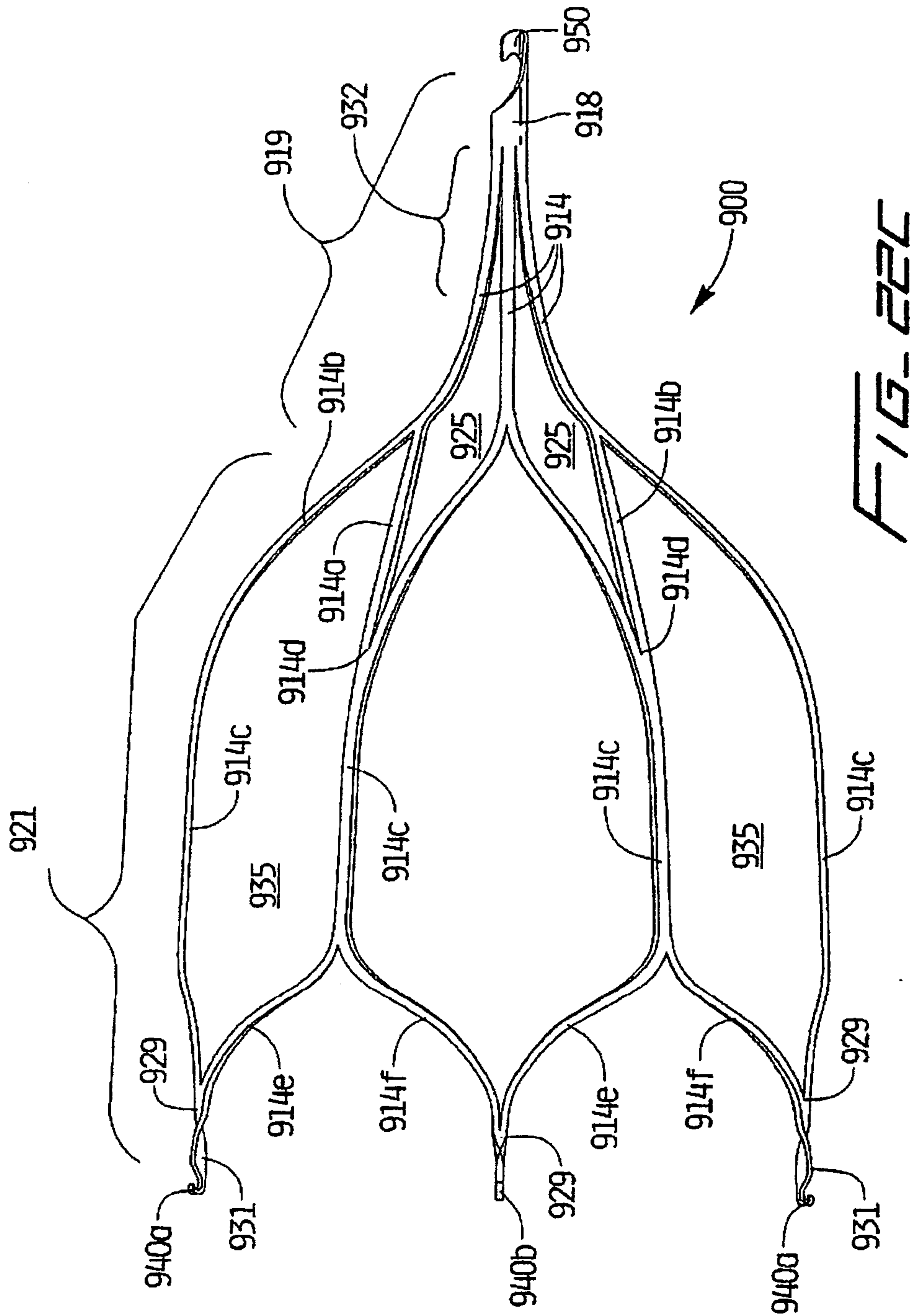


FIG. 22C

940b
929
940a
929

FIG. 220

914c
914c

900

914
918
950

FIG. 222E

940a
929
940b
914e
914f
914e
914f
929
931
940b
940a

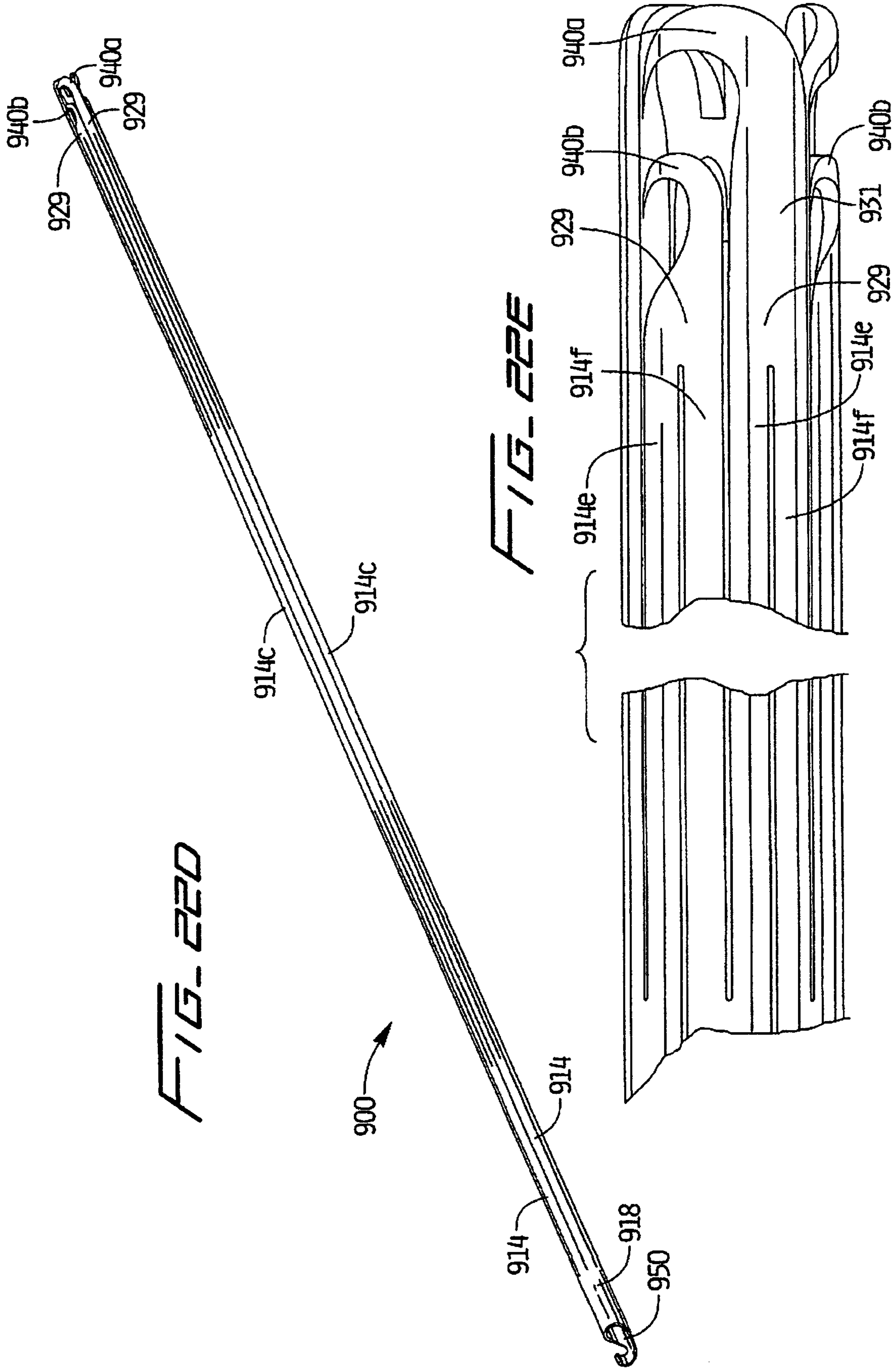


FIG. 23

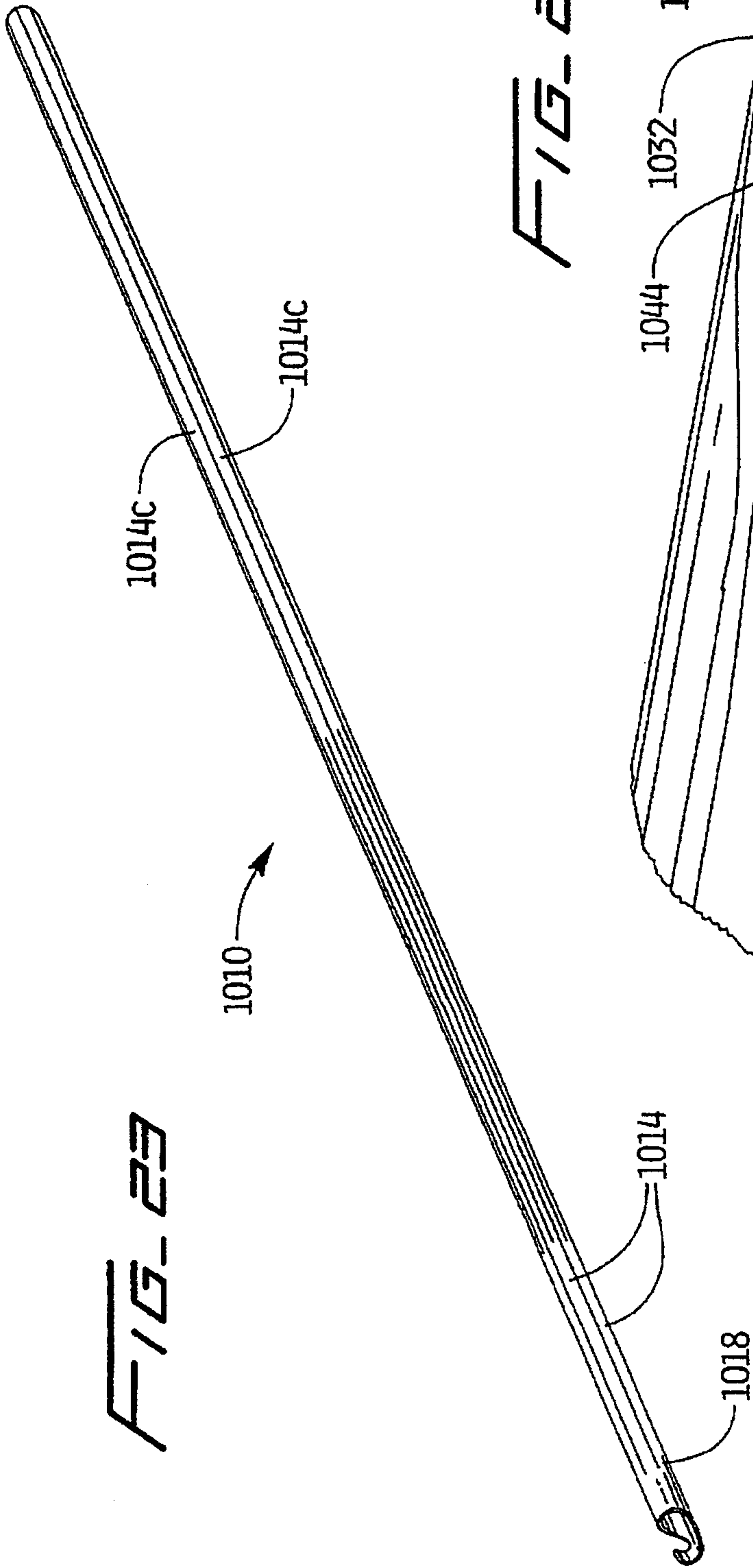
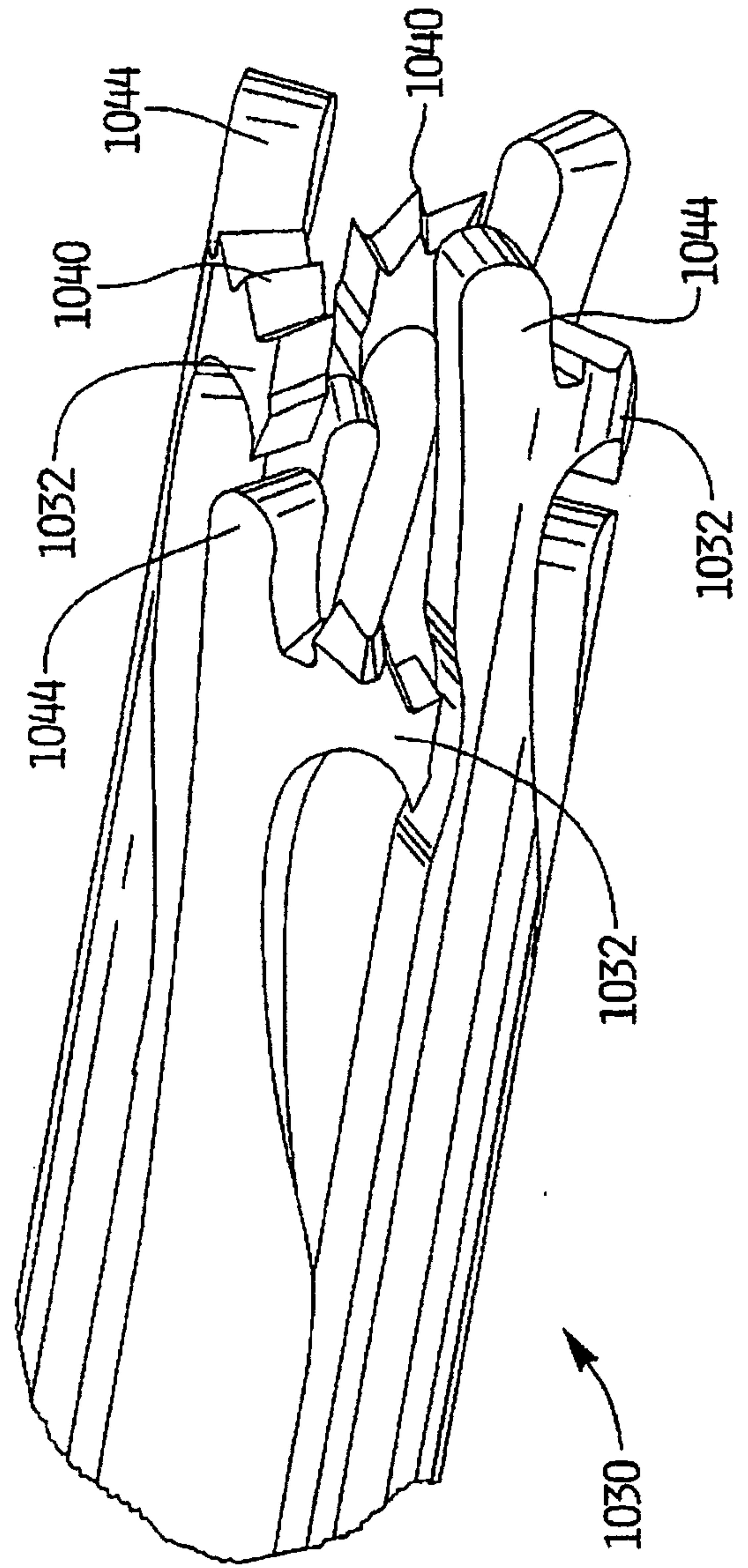


FIG. 24



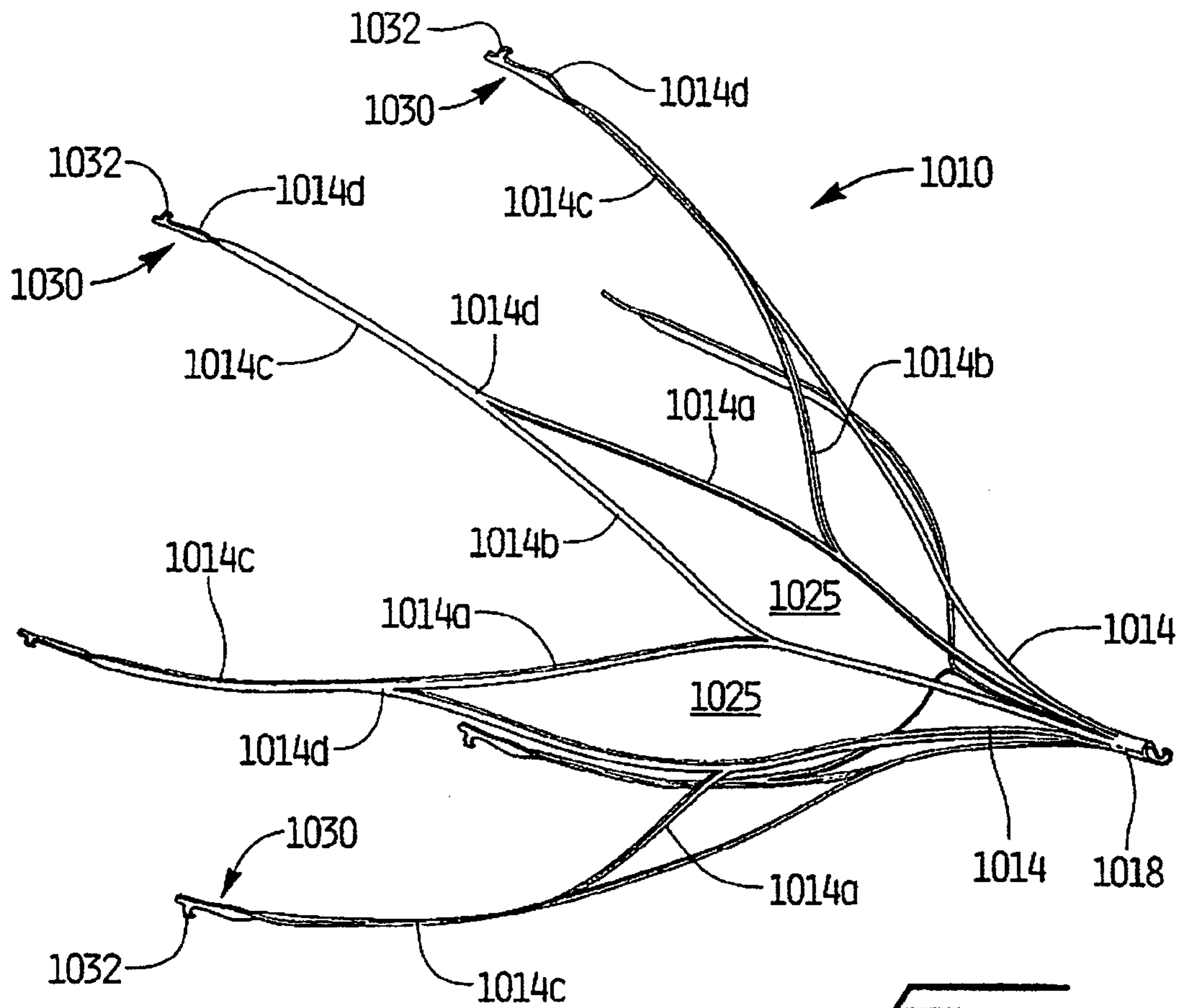


FIG. 25

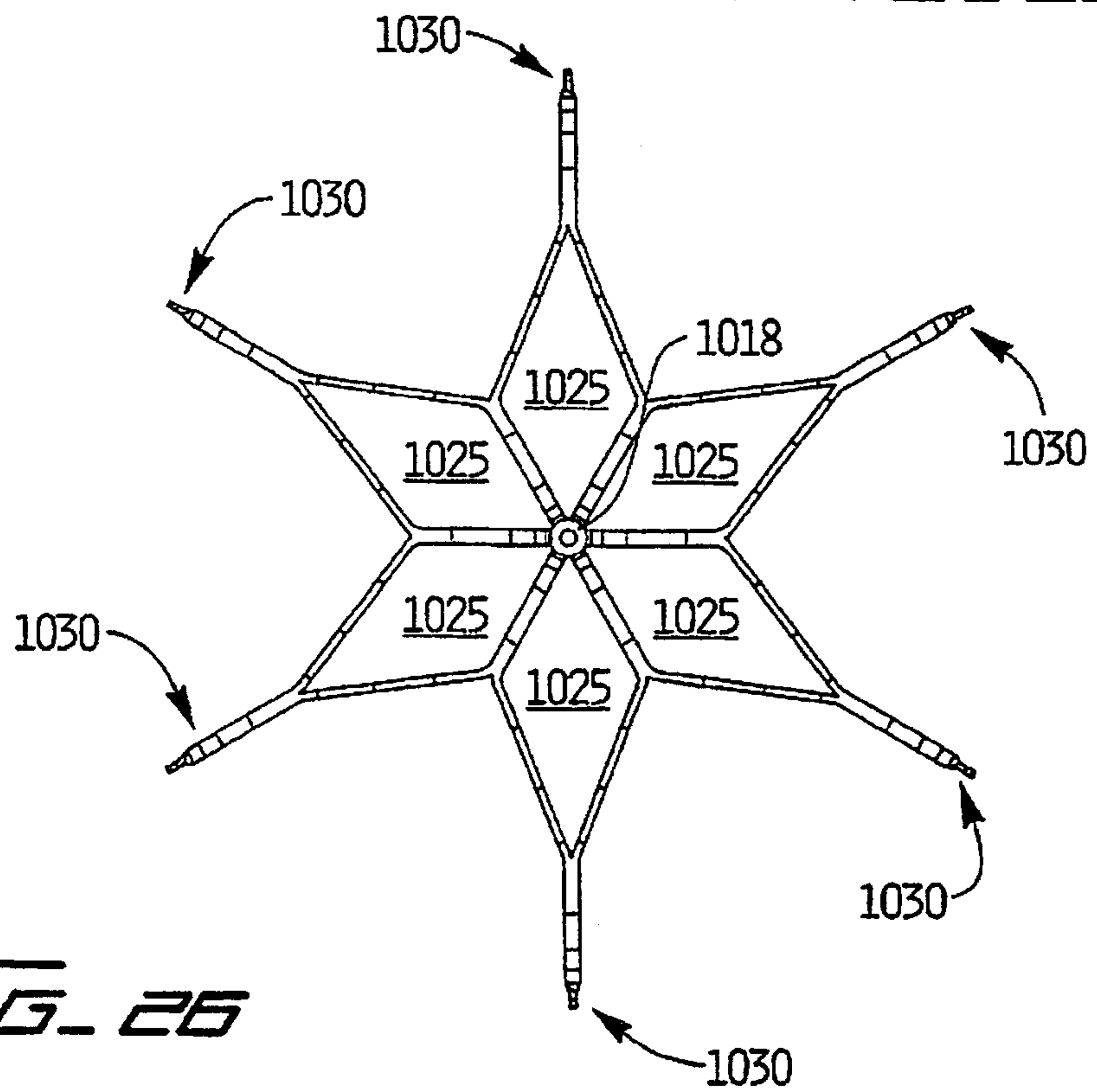


FIG. 26

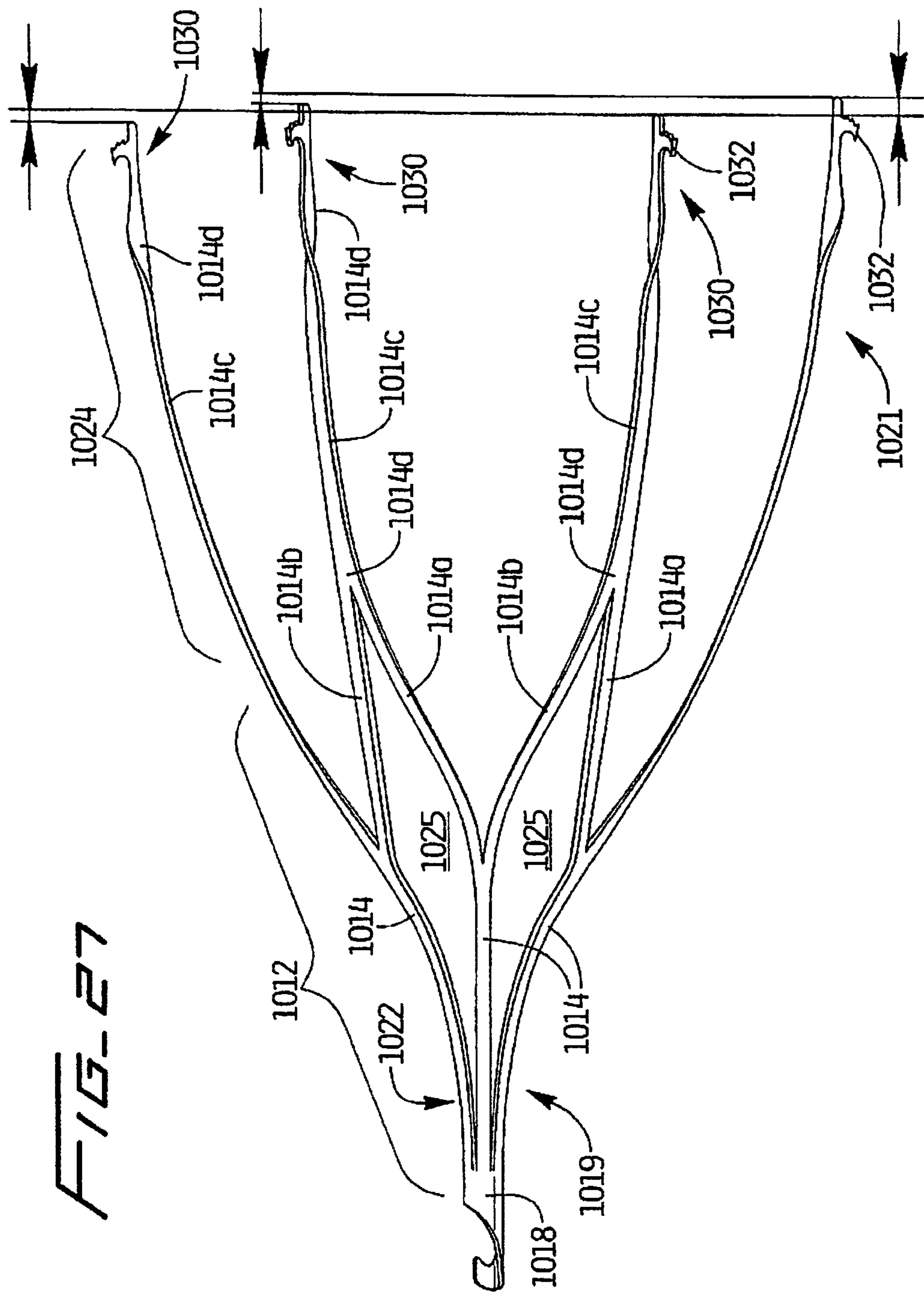


FIG. 27

