

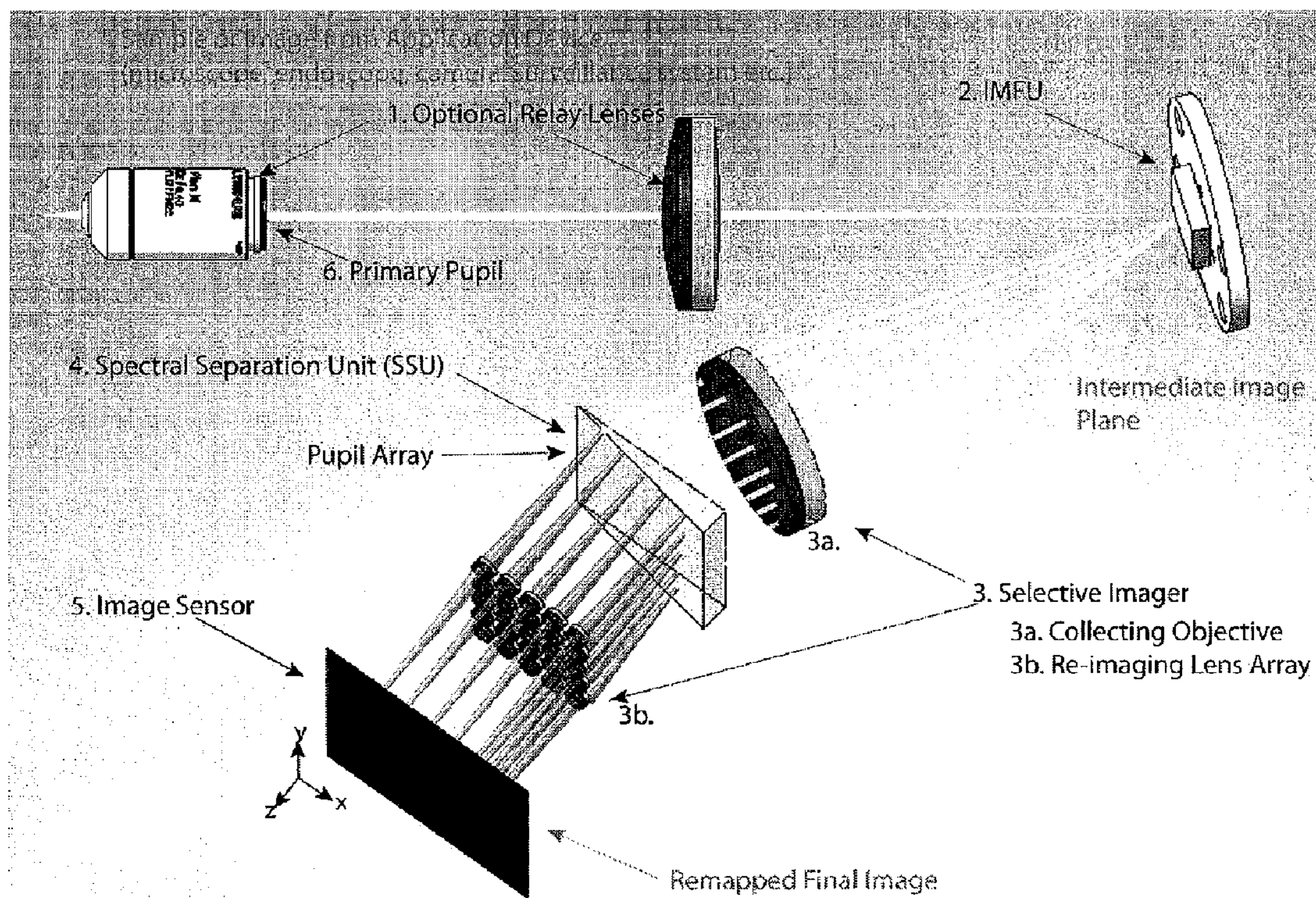


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(54) Title: IMAGE MAPPING SPECTROMETERS

Fig. 2



(57) Abrégé/Abstract:

Devices and methods for hyperspectral and multispectral imaging are discussed. In particular, Image Mapping Spectrometer systems, methods of use, and methods of manufacture are presented. Generally, an image mapping spectrometer comprises an

(57) **Abrégé(suite)/Abstract(continued):**

image mapping field unit, a spectral separation unit, and a selective imager. Image mapping spectrometers may be used in spectral imaging of optical samples. In some embodiments, the image mapping field unit of an image mapping spectrometer may be manufactured with surface shaped diamond tools.

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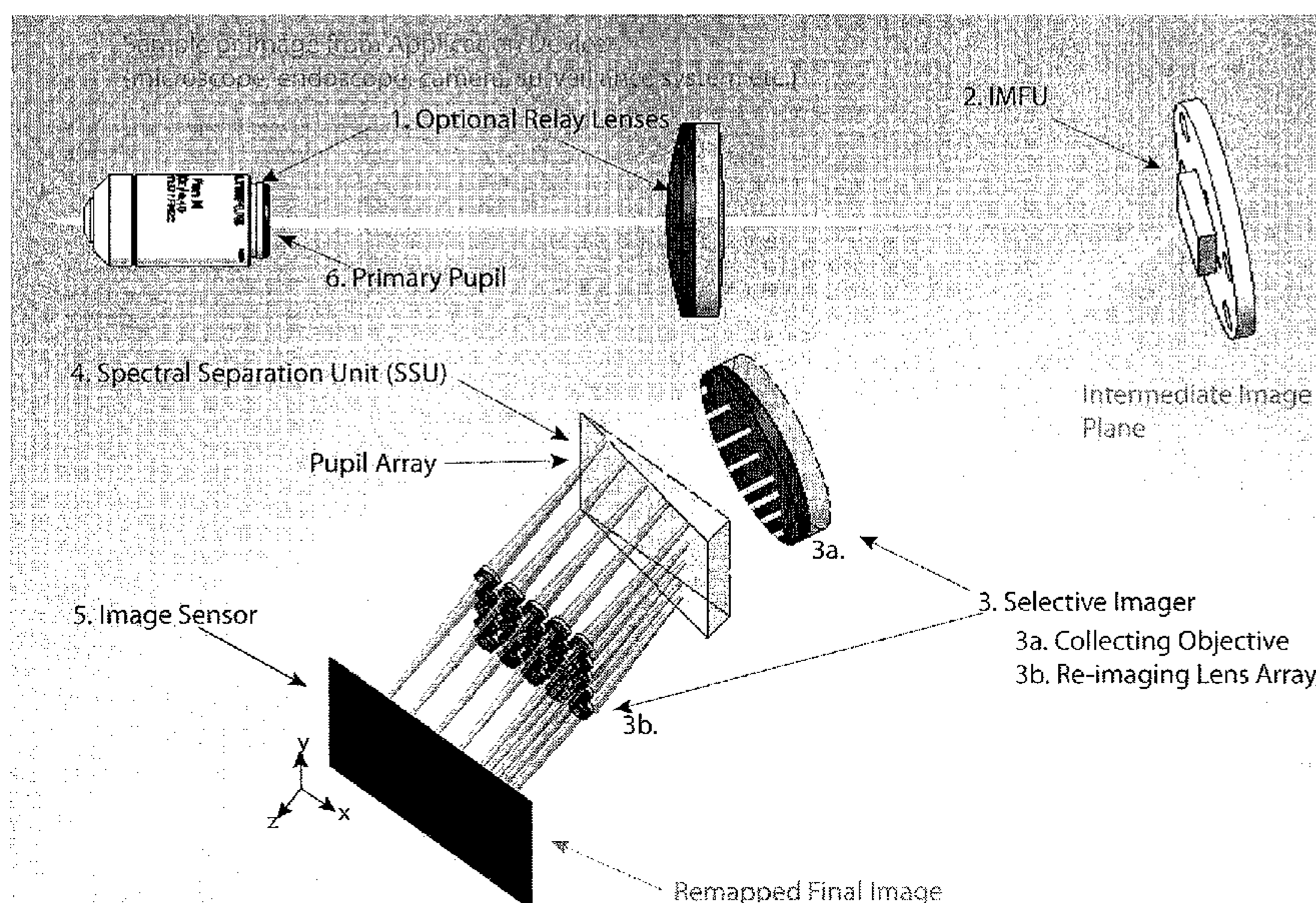
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Fig. 2



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IMAGE MAPPING SPECTROMETERS

CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This application claims benefit of U.S. Provisional Patent Application Serial No. 61/111,182, filed November 4, 2008, which is herein incorporated by reference.

BACKGROUND

[0002] A hyperspectral imager is a known device that is commonly used to examine the spectral, or wavelength dependent, content of an object or scene. (Hyperspectral imagers are also referred to as imaging spectrometers.) In a hyperspectral imager, light emitted or reflected by a given object or scene is imaged onto the entrance of a spectrometer, usually a slit element that transmits a single line image of the object or scene. The spectrometer in turn re-images this light to another location while dispersing this light according to its wavelength in a direction orthogonal to the orientation of the slit element, where it can readily be observed or recorded. In this manner, each line image of the object or scene is decomposed into a two-dimensional data array, and by scanning the object or scene in line-by-line increments, a three-dimensional datacube is formed.

[0003] Fluorescence microscopy is used extensively to gain a deeper understanding of varying cellular dynamics. A major impetus towards the widespread application of this analytical tool is the ongoing development of fluorescent proteins, nanocrystals, and organic fluorophores with a range of sensitivities for physiological analytes. Development and application of fluorescent probes has revolutionized studies of cell and tissue physiology. However, to fully utilize the potential information yielded by these probes, detection systems must simultaneously monitor the spectroscopic variations of a combination of fluorophores. This requirement comes from the fact that most cellular responses do not occur in isolation, rather there is a complex sequence of events that occurs in response to cellular effectors. Furthermore, samples of physiological interest often consist of a heterogeneous population of cells, each potentially coupled to other cells and responding to a perturbation with a unique pattern. In order to determine the time sequence of such events with fluorescence techniques, a spectral imaging system must exhibit an appropriate combination of high spatial, spectral, and temporal resolution. Due to the scanning requirements of currently available systems, one or more of these parameters is often sacrificed for the improvement of another. This leads to spatial or temporal ambiguities in the time course of biological processes. These same limitations are also present for endogeneous fluorescence signals where there are often

unique combinations of different molecules in the sample with unique temporal interactions that are difficult to detect with scanning techniques. In addition, many endogeneous and exogenous fluorescence contrast agents photobleach over time and would benefit from non-scanning approaches that can collect the signal over the full integration period. Reflectance and absorption based signals also experience similar detection tradeoffs with scanning based imaging spectrometers.

[0004] A growing trend in endoscopic imaging techniques for early and pre-cancer detection has been to enhance their diagnostic capabilities by improving the spectral content of their images. Spectroscopy techniques have demonstrated that endogenous cancer bio-markers such as nicotinamide adenine dinucleotide (“NADH”), flavin adenine dinucleotide (“FAD”), collagen, and oxy- and deoxy-hemoglobin have distinct fluorescence and reflectance based spectral signatures. These molecular bio-markers may serve as important indicators in identifying pre- and early cancerous regions to more traditional morphologic and architectural features. Imaging spectrometers have been proposed but drawbacks have limited their use as affordable, real-time screening tools. The main limitation of these approaches has been their reliance on expensive tunable filters, such as liquid crystal or acousto-optic, for acquiring the increased spectral bandwidth. Not only are these filters prohibitively expensive, but they also delay imaging acquisition times (> about 23 seconds) due to the serial fashion in which the spectral data is collected. Snapshot techniques such as the Computed Tomography Imaging Spectrometer (“CTIS”) avoid this limitation, however these have long post-acquisition processing (about 30 to 60 min) which is also ill-suited for *in vivo* imaging.

[0005] Remote sensing is a valuable tool for acquiring information from dangerous or inaccessible areas such as war zones, glaciers, ocean depths, hurricanes, gas plumes, biological weapons, etc. Imaging spectrometers enhance remote sensing techniques providing critical information based on subtle spectral features from a sample. These devices are often used on vehicles that travel at high speeds, such as satellites and planes, consequently requiring fast data collection. Scanning-based approaches often compromise on image size, contrast, and/or spectral resolution to meet these fast temporal acquisition requirements. In some cases, the event in question, such as verification that a missile has hit its target, transpires so fast that it is virtually impossible for scanning approaches to be used, such as verification that a missile has hit its target. Therefore, non-scanning, snapshot spectral imaging techniques would be desirable.

[0006] Food inspection plays an important role in assuring the quality of the food that is consumed within our country. However, this process is typically a human-based manual observation of the food for visually-apparent defects. This approach has several limitations, including the fact that many defects are not observable with the human eye. It can also be a slow process, prone to human errors and sampling inaccuracies. Spectral imaging techniques can play a significant role in this area by being able to evaluate food for multiple defects in a quick and quantitative manner based on unique spectral signatures. To have minimal impact on the time to market, these inspection stations must acquire and analysis information very fast, limiting the usefulness of scanning based approaches.

SUMMARY

[0007] The present disclosure is generally in the field of hyperspectral and multispectral imaging. More particularly, the present disclosure, according to certain embodiments, relates to compact Image Mapping Spectrometer (“IMS”) systems and methods.

[0008] One embodiment of the present disclosure provides an image mapping spectrometer. The image mapping spectrometer comprises an image mapping field unit. The image mapping spectrometer further comprises a spectral separation unit. The image mapping spectrometer further comprises a selective imager.

[0009] Another embodiment of the disclosure provides a method of spectral imaging. The method of spectral imaging comprises providing an optical sample. The method of spectral imaging further comprises providing an image mapping spectrometer, wherein the image mapping spectrometer comprises an image mapping field unit, a spectral separation unit, and a selective imager. The method of spectral imaging further comprises imaging the optical sample with the image mapping spectrometer.

[0010] Yet another embodiment of the disclosure provides a method of fabricating image mapping field units. The method of fabricating image mapping field units comprises providing an image mapping field unit substrate. The method further comprises providing an optical component cross section profile. The method further comprises providing a surface shaped diamond tool specific to the optical component cross section profile. The method further comprises utilizing the surface shaped diamond tool to create the optical component cross section profile in the image mapping field unit substrate to form a mapping element.

[0011] The features and advantages of the present invention will be apparent to those skilled in the art. While numerous changes may be made by those skilled in the art, such changes are within the spirit of the disclosure.

DRAWINGS

[0012] Some specific example embodiments of the disclosure may be understood by referring, in part, to the following description and the accompanying drawings.

[0013] Figure 1 illustrates an imaging sequence of 3D Object Cube to charge-coupled device (“CCD”) array according to one embodiment of an Image Mapping Spectrometer (“IMS”) system.

[0014] Figure 2 illustrates the basic configuration for an IMS system, according to an embodiment of the disclosure.

[0015] Figure 3 illustrates examples of possible image mapping field unit (“IMFU”) designs, according to embodiments of the disclosure.

[0016] Figure 4 illustrates a diamond machining configuration (raster fly cutting) for fabrication of IMFUs using design-specific surface-shaped diamond tools, according to embodiments of the disclosure.

[0017] Figure 5 illustrates a multi-faceted surface-shaped diamond tool, according to embodiments of the disclosure.

[0018] Figure 6 illustrates a fabrication-related aberration known as “edge-eating,” typically caused by diamond machining in raster-fly cutting.

[0019] Figure 7 presents IMFU several design configurations that may minimize the effect of edge-eating, according to embodiments of the disclosure.

[0020] Figure 8 illustrates (a) simulated diffraction effects caused by the miniature optical components in an IMFU, and (b) optimum placement of an adjacent sub-pupil for minimum crosstalk of approximately 1%, according to embodiments of the disclosure.

[0021] Figure 9 illustrates (a) an image created by an actual pupil from an IMS system, according to embodiments of the disclosure, with 25 tilts (5 x-tilts and 5 y-tilts), and showing the elliptical pupil caused by diffraction. This is compared to the image created by a simulated pupil (b). Cross sections through the y-axis and x-axis of actual and simulated pupils are shown in (c) and (d), respectively.

[0022] Figure 10 illustrates different Selective Imager configurations for the lens array component, according to embodiments of the disclosure.

[0023] Figure 11 illustrates results from a simulation, verifying the chromatic aberration correction for the Selective Imager using optical modeling software, according to embodiments of the disclosure.

[0024] Figure 12 illustrates results from a simulation, verifying the spectral separation for the ISM system at the final image plane using optical modeling software, according to embodiments of the disclosure.

5 [0025] Figure 13 illustrates one example of an image mapper that has three tilt angles for the y-axis and three for the x-axis, according to an embodiment of the disclosure. The total number of tilts is 9, which corresponds to number of sub-systems of the Selective Imager, and also relates to the separation between image lines at the surface of image sensor.

[0026] Figure 14 illustrates a single axis tilted image mapper, according to one embodiment of the disclosure.

10 [0027] Figure 15 illustrates a reflective IMS system with annular mirror, according to one embodiment of the disclosure.

[0028] Figure 16 illustrates a reflective IMS system with beam splitter, according to one embodiment of the disclosure.

15 [0029] Figure 17 illustrates a reflective and tilted IMS system, according to one embodiment of the disclosure.

[0030] Figure 18 illustrates a refractive IMS system, according to one embodiment of the disclosure.

[0031] Figure 19 illustrates an array of IMS lenses, according to one embodiment of the disclosure.

20 [0032] Figure 20 illustrates a multi-spectral, or "increased range," IMS system, according to one embodiment of the disclosure.

[0033] Figure 21 illustrates a multi-spectral, or "increased spectral range," IMS system using a single image detector, according to one embodiment of the disclosure.

25 [0034] Figure 22 illustrates an increased spectral sampling IMS system using field compressing components, according to one embodiment of the disclosure.

[0035] Figure 23 illustrates a dynamic IMS system, according to one embodiment of the disclosure.

[0036] Figure 24 illustrates a waveguide IMS, according to one embodiment of the disclosure.

30 [0037] Figure 25 illustrates an IMS system with multiple IMFUs, according to one embodiment of the disclosure.

[0038] Figure 26 illustrates an IMS system which may be well suited for endoscopic applications, according to one embodiment of the disclosure.

[0039] Figure 27 illustrates an IMS system which may be well suited for ophthalmic applications, according to one embodiment of the disclosure

[0040] Figure 28 illustrates an example IMS system setup at the side port of an inverted microscope, according to one embodiment of the disclosure.

5 [0041] Figure 29(a) shows an early IMFU, according to an embodiment of the disclosure. Figure 29(b) shows the IMFU of Figure 29(a) with a US Nickel for size reference. Figure 29(c) illustrates a Zygo NewView 5000 3D image of the center region of ramp mirrors 1-5 of IMFU of Figure 29(a); the false color shows depth information.

10 [0042] Figure 30 illustrates images that results from the example system in Figure 28. Figure 30(a) illustrates a single sub-image of a 1951 USAF resolution test target; Figure 30(b) illustrates a 1X5 pupil image; Figure 30(c) illustrates an image from a halogen source; and Figure 30(d) illustrates the spectral spread from source image spatial mapping lines.

15 [0043] Figure 31 illustrates an early IMS system, according to an embodiment of the disclosure. The IMS system may be capable of collecting a 3D (x, y, λ) datacube of 100 X 100 X 25 in a single integration event. Figure 31(b) illustrates a schematic of the IMS system.

[0044] Figure 32 illustrates overlap of the field of views ("FOVs") on the CCD camera, according to embodiments of the disclosure. The FOVs of adjacent reimaging lenses may overlap to fully utilize the CCD area.

20 [0045] Figure 33 illustrates a 1951 USAF resolution test target undispersed image, according to certain embodiments of the disclosure. The raw image (a) may be obtained using a 16-bit camera without binning (pixel size $\sim 9 \mu\text{m}$). Figure 33(b) illustrates the reconstructed image. For comparison purposes, an image of the same bars is captured at the microscope side port directly using a monochromatic camera, as shown in (c). The top bars in the FOV belong to Group 7, Element 6 (bar width $\sim 2.19 \mu\text{m}$).

25 [0046] Figure 34 illustrates the point spread function of a single mapping line from an undispersed image, according to an embodiment of the disclosure. The camera pixel size equals $9 \mu\text{m}$. The x and y positions indicate the location in the image in the CCD camera's global coordinates.

30 [0047] Figure 35 illustrates IMS images from a 100 X 100 X 25 system of green fluorescent beads, according to an embodiment of the disclosure. The raw image may be obtained using a 16-bit CCD camera with about 6 s integration time. The bead's spectrum may be obtained from point A in the reconstructed image.

[0048] Figure 36 illustrates IMS images of red and yellow fluorescent beads, according to an embodiment of the disclosure. The raw image may be obtained using a 16-bit CCD camera with about 2 s integration time. The yellow bead's spectrum may be from point B in the reconstructed image, and the red bead's spectrum may be from point C in the reconstructed image.

[0049] Figure 37 illustrates a picture of an early IMS system, according to an embodiment of the disclosure. The IMS system may be capable of collecting a 3D (x, y, λ) datacube of 285 X 285 X 62 in a single integration event. The schematic for this system is similar to Figure 31(b).

[0050] Figure 38 (side) illustrates a biological sample imaged with a reference CCD. The biological sample comprises bovine pulmonary artery endothelial cells incubated with MitoTracker[®] Red CMXRos to label the mitochondria, BODIPY[®] FL phalloidin to label the filamentous actin (F-actin), and 4',6-diamidino-2-phenylindole ("DAPI") to label the nucleus. Figure 38 (bottom) illustrates 28 spectral band images of the biological sample with about 5-8 nm spectral spacing from about 500 – about 684 nm taken with IMS system, according to an embodiment of the disclosure.

[0051] Figure 39(a) illustrates a Nanotech 250 UPL Machine with axis labeled for manufacturing an IMFU, according to embodiments of the disclosure. Figure 39(b) illustrates a close up of a goniometer fixture used to rotate the IMFU for -fabrication of x-tilt mirror facets.

[0052] Figure 40(a) illustrates a top view of a large format IMFU, having 285 mirror facets and 25 tilts in the x- and y-axis, with a US Quarter for size comparison, according to an embodiment of the disclosure. Figure 40(b) illustrates a side view close-up of the large format IMFU of Figure 28(a).

[0053] Figure 41 illustrates white light interferometer surface profile measurements of individual mirror facets in a large format IMFU taken at the (a) left edge, (b) center, (c) right edge of the component, according to an embodiment of the disclosure.

[0054] Figure 42 displays typical roughness results obtained from a large format IMFU (285 mirror facets) fabricated using a 75 micron wide surface shaped diamond tool, according to an embodiment of the disclosure.

[0055] The patent or application file contains at least one drawing executed in color. Copies of this patent or patent application publication with color drawing(s) will be provided by the Office upon request and payment of the necessary fee.

[0056] While the present disclosure is susceptible to various modifications and alternative forms, specific example embodiments have been shown in the figures and are herein described in more detail. It should be understood, however, that the description of specific example embodiments is not intended to limit the invention to the particular forms disclosed, but on the contrary, this disclosure is to cover all modifications and equivalents as illustrated, in part, by the appended claims.

DESCRIPTION

[0057] The present disclosure is generally in the field of hyperspectral and multispectral imaging. More particularly, the present disclosure, according to certain embodiments, relates to compact Image Mapping Spectrometer (“IMS”) systems and methods.

[0058] In the context of this document, the term “mapping” generally refers to a process by which data is transformed to form a final image. In a typical imaging system, a mapping transformation may be linear, often having axial symmetry. Mappings may also include any process that may be of a certain arrangement or orientation, thereby enabling spectral and spatial information to be collected in parallel.

[0059] As used herein, a “lens” generally refers to any optical component or combination of multiple optical components with a combined optical power. A lens may comprise one or more refractive components, one or more diffractive components, one or more reflective components, and any combination of refractive, diffractive, and/or reflective components.

[0060] As used herein, a “mapping line” generally refers to a 1-dimensional collection of points, either through the entire optical sample or a portion of the optical sample. A “mapping pixel” generally refers to a single point from any location within the optical sample. A “mapping region” generally refers to a 2 dimensional, contiguous collection of points, either through the entire optical sample or a portion of the optical sample. A “tilt” generally refers to the direction that the chief ray, or center optical ray, propagates to or from a point within the optical sample.

[0061] As used herein, an “aperture stop,” or “stop,” generally refers to a physical component that limits a bundle of light from an axial point in an optical sample. An image of the stop in any optical space in the optical system may be referred to as a “pupil.” In some cases, the stop of an optical component may be referred to as the pupil, as they are conjugate images of one another, and they serve the same function for that example.

[0062] The present disclosure provides, according to certain embodiments, an Image Mapping Spectrometer (IMS) useful for hyper- and multispectral imaging based on image mapping principles. Devices and methods of this disclosure may be applied to biological and medical imaging, bio-computing, surveillance applications, remote sensing (for example missile defense, detection of improvised explosive devices, field detection, bio-chemical detection), atmospheric imaging (for example in meteorology or pollution screening), food inspection, and numerous other applications requiring real time spectral imaging (for example, Raman Spectroscopy, coherent anti-Stokes Raman scattering (“CARS”), and Spectro-Polarimetry and Polarimetry). An IMS may acquire spectral information instantaneously, without the need for scanning. An IMS may acquire a great deal of image and spectral data in parallel. For example, an IMS may acquire about 1 million voxels at once. In some embodiments, an IMS may acquire about 5.2 million voxels at once, while other embodiments may provide for simultaneous acquisition of between about 16 million and about 100 million voxels. An IMS may transmit image data to remote locations, for example, locations separated by great distances (longer than about 10 m) and/or locations which do not allow line-of-sight viewing. Advantages of a scanless system include, for example, high optical throughput, fast image acquisition, and high spectral/spatial correlation. To create an image, an IMS may require very limited processing (image re-mapping), thereby providing a fast, unambiguous, and straightforward procedure. There are several applications in which this is beneficial; one such application is in the area of fluorescence spectral imaging for simultaneous high-resolution sub-cellular microscopy of multiple fluorescence probes in living cells.

[0063] The present disclosure also provides, according to certain embodiments, an IMS coupled with one or more other imaging systems such as, for example, microscopes, endoscopes, point-of-care (“POC”) devices, cameras, night-vision instruments, and the like. An IMS also may be applied to any electromagnetic radiation, for example, spectral bands from ultraviolet, visible, and infrared radiation. It also may be possible to combine spectral ranges such as: visible and near infrared, midwave infrared, long-wave infrared, and many other regions to create multi-band implementations.

[0064] The present disclosure also provides, according to certain embodiments, a spectral imaging method capable of acquiring full spectral information simultaneously on an array detector or a combination of array detectors (for example a IMS may use a large format detector or several detectors). Without limiting the invention to a particular theory or mechanism of action, it is nevertheless currently believed that an IMS works by spatially

redirecting image mapping regions to obtain space between the detectors/pixels. Then, through the use of diffractive, refractive, and/or combined components, an IMS may fill this space with spectral information from these redistributed image zones. This final spatially and spectrally redistributed image may be detected and/or recorded by an Image Sensor (for example a charge-coupled device (“CCD”), complementary metal oxide semiconductor (“CMOS”), array of photodiodes, avalanche photodiodes, array of photomultiplier tubes, thermal detectors, and others), thereby providing unambiguous 3-dimensional (x, y, λ) information (sometimes referred to as a “datacube”) on the Image Sensor.

[0065] By way of explanation, and not of limitation, the operating principle of the proposed IMS instrument is shown in Figure 1. As an example, consider a simple optical sample which consists of 4 spectral bands with no color overlap for various object points (Figure 1A). First, selected rows of a 3D (x, y, λ) object may be shifted and imaged onto a large format Image Sensor to create an area for spectral spread (Figure 1B). This area is represented in the figure with white squares (individual detectors of an Image Sensor). After the row shifts, they may be dispersed into the perpendicular direction to allow acquisition of 3D (x, y, λ) information in a single image (Figure 1C). In other words, spatial and spectral information may be encoded in a single snapshot, and every spatial-spectral component may be mapped to a different detector of an Image Sensor. The significance of such an approach becomes profound for objects with numerous spectral bands at the same spatial location. (An example of such an object is shown in Figure 1D.) Using traditional imaging, several wavelength bands may be integrated by the same detector, and the spectral signature may be lost (Figure 1E), while it is preserved with the IMS mapping techniques (Figure 1F).

[0066] Note that the total number of x, y , and λ elements typically will not exceed the total number of detectors on the Image Sensor to provide unambiguous and direct spatial-spectral information. As used herein, “unambiguous” generally refers to a direct, one-to-one correspondence between the smallest data volume, commonly called a voxel, from the 3D (x, y, λ) datacube, and the individual detectors, from the 2D Image Sensor. For example, a 1024 x 1024 detector Image Sensor can acquire 256 x 256 x 16 or 512 x 512 x 4 datacubes unambiguously, where the first two numbers denote the quantity of spatial elements in the x and y directions, and the third number represents the number of spectral bands. After image acquisition, the data may be re-mapped and processed (commonly with the use of certain computers and/or software) to display a live color image on the computer screen from which a spectrum can be obtained in real time at each mapping pixel. Note that ambiguous data can also

be collected to further enhance the spatial/spectral sampling; however this may require image processing techniques and may, therefore, result in slower image display.

[0067] In general, an IMS of the present disclosure comprises an Image Mapping Field Unit (“IMFU”), a Spectral Separation Unit (“SSU”), and a Selective Imager. An IMS may be designed as an autonomous instrument that can be used on its own or combined with other research or diagnostic tools (inverted microscope, endoscope, and the like). A conceptual view of an example IMS layout is presented in Figure 2. Therein, an optical sample (not shown) is imaged by the IMS. The optical sample may be a physical object, an image from a pre-imaging system, or a conjugate image of either. The optical sample may provide electromagnetic radiation for IMS imaging through any mechanism, such as transmission, reflection, or fluorescence. The electromagnetic radiation may be first collected through a primary pupil 6. The primary pupil 6 may be preceded and/or followed by one or more optional relay lenses 1. In the embodiment shown in Figure 2, an optional relay lens 1 both precedes and follows the primary pupil 6. An optional relay lens may be any optical component which is capable of relaying an image from the optical sample to the IMFU. For example, an optional relay lens may be a lens, an array of lenses, a gradient-index (“GRIN”) lens, an optical fiber or a bundle of optical fibers. (Fiber optic optional relay lenses may be especially beneficial in endoscopic applications.) The electromagnetic radiation then impinges upon the IMFU 2. As will be discussed further below, the IMFU 2 spatially reorganizes the image, also called “image mapping” or “mapping,” as it redirects the electromagnetic radiation towards the Selective Imager 3. The IMFU may be located generally at any virtual or real image conjugate location, or field space, or within a millimeter or less from an image conjugate location. The Selective Imager 3 generally comprises two spatially separated components: (1) a collecting objective or array of collecting objectives 3a, and (2) an array of re-imaging lenses 3b. As shown in Figure 2, the SSU 4 may be positioned between the two components of the Selective Imager 3. The SSU may be located generally at any pupil conjugate location, or aperture space, or within several millimeters or more from a pupil conjugate location. For example, the SSU 4 may be positioned between the primary pupil 6, and the IMFU 2, between the IMFU 2 and the Selective Imager 3, or between the Selective Imager 3 and the Image Sensor 5. Finally, the electromagnetic radiation may impinge upon the Image Sensor 5. The Image Sensor 5 may comprise any array of sensing units or detectors capable of quantitatively measuring electromagnetic radiation, such as a CCD. It should be understood that, for simplicity, this disclosure may discuss or illustrate any given optical component as a lens or a prism, but each component may comprise multiple

lenses or prisms to achieve the desired effect. As used herein, the “configuration” of an IMS generally refers to the number, type, and layout of elements (including the optical sample, primary pupil, optional relay lenses, IMFU, Selective Imager collecting objective, Selective Imager re-imaging lens array, SSU, and Image Sensor) with respect to one another.

5 [0068] An IMFU, or mapper, spatially reorganizes an image to create optically void regions in the image space used for encoding spectral information. An IMFU may comprise optical components spatially distributed on its face. Certain distributions may exhibit similar optical functions, thereby forming logical groupings of optical elements. For example, mapping regions 1, 4, and 7 may exhibit similar optical functions, and may be logically grouped
10 as IMFU optical component group A; while mapping regions 2, 3, 8, and 9 may exhibit similar optical functions, different from those in IMFU optical component group A, and mapping regions 2, 3, 8, and 9 may be logically grouped as IMFU optical component group B. In some embodiments, the IMFU optical component groups may be distributed symmetrically on the face of the IMFU. In some embodiments, the distribution of IMFU optical component groups may
15 form geometric shapes and/or repeating patterns. The optical components may be spatially distributed in particularly useful mapping shapes, such as mapping lines, mapping pixels, and/or mapping regions, although other common shapes (e.g., square, triangle, “L”, “O”, etc.) may also be used. The optical components of a particular mapping line, mapping pixel, and/or mapping region may, therefore, exhibit similar optical functions specific to that shape. The distribution of
20 IMFU optical component groups in other embodiments may be random or chaotic. The image created by an optical component group may be referred to as a sub-image. The particular distribution of IMFU optical component groups on the face of the IMFU may be referred to as the “geometry” of the IMFU. As would be understood by one of ordinary skill in the art with the benefit of this disclosure, the geometry of an IMFU uniquely defines the mapping. Moreover,
25 the geometry of the IMFU may be static or dynamic, and the geometry may be controlled and varied in real-time without disassembly of the system or disturbance of the optical sample.

[0069] The IMFU optical components may redirect the chief ray from object points to new locations in the image. The IMFU optical components may be refractive, reflective, or waveguide. Refractive approaches may include, for example, arrays of prisms,
30 lenses, and/or combination optical components. Reflective approaches may include, for example, arrays of mirrors and/or lenses, as in a catadioptric approach. Waveguide approaches may include, for example, fiber optics. Any type of mapper also may possess optical power, similar to a more traditional field lens or mirror, and may be capable of re-imaging an exit pupil

from the relay optical system to the Selective Imager collecting objective's entrance pupil or array of collecting objective pupils. This may allow for a compact and optically efficient multi-imaging system. The mapper may also incorporate anamorphic or cylindrical curvature for each mapping component, which may enhance the spectral resolution of the system. Lastly, the IMFU may combine refractive and reflective components to perform these different tasks individually or in combination. The IMFU may be corrected for spectral separation.

[0070] Figure 3 shows several examples of possible IMFU designs. For the purpose of the following discussion, only 9 unique tilt angles are discussed; however, in practice many more tilt angles may be used. Additionally, only mirror components are illustrated, while IMFU components may also include, for example, prisms, lenses, and combination optical components. The geometry in Figure 3(a) illustrates redirection of entire horizontal mapping lines through the object into 9 different angular directions. Rotation may be performed around two x and y axes to provide large spectral sampling and/or resolution of the system. This approach may be advantageous in its simplicity in concept and fabrication. However, this approach may suffer in that, for larger tilted mirrors, the image being mapped may go out of focus, thereby decreasing the spatial resolution at the edge of the field. This disadvantage may be reduced in the second geometry shown in Figure 3(b), wherein the image mapping line may be broken into 2, 3, or more segments in the horizontal (x-axis). This geometry may have better mapping performance but might be more difficult to fabricate. The third exemplary IMFU geometry, shown in Figure 3(c), is a mapping pixel-sized mirror approach, either static or active (e.g., MEMS mirrors, liquid crystal modulator, and the like). This concept is versatile and may provide any number of remapping schemes for recording both spectral and spatial information. Note that mapping pixels do not need to be square or rectangular. An example of a circular mapping pixel mapper is illustrated in Figure 3(d) and is conceptually similar to that shown in Figure 3(c). In addition to tilted mapping components, each tilt mirror facet may also have optical power for focusing the reflected (or refracted) light. This focusing effect may be used for compressing the image mapping pixel size, thereby increasing the spectral sampling of the system, as shown in Figure 3(e). The entire IMFU may also have optical power and may be used for re-imaging the exit pupil of the fore optics in the system, as illustrated in Figure 3(f). In Figure 3(g), a combination of two or more element mappers also may be used, combining tasks either individually or collectively for image mapping purposes.

[0071] As mentioned above, IMFUs may be refractive or reflective. A refractive IMFU may be similar in geometry to a reflective IMFU, but a refractive IMFU may redirect the

optical samples mapping pixel's chief ray as the light is transmitted through, not reflected from, the surface. Both refractive and reflective types may be used statically or dynamically. For example, dynamic microelectromechanical system ("MEMS") mirror arrays may be developed that function similar to a digital light processor ("DLP") device that may be used in high definition televisions ("HDTV"). For example, a suitable DLP may be commercially available from Texas Instruments of Dallas, Texas. The main drawback of existing DLPs for this application is that they are limited to only two possible positions (on and off), and therefore cannot provide enough flexibility for real time adjustment of spatial/spectral resolutions. Accordingly, an analog or high bit depth array, with several tilt positions in yaw and pitch to redirect individual optical sample mapping pixels to any region in the image plane to maximize applicability, may be used. Other examples of a dynamic IMFU may also include liquid crystal modulators and refractive liquid modulators (micro fluidic based). Such mappers may be combined with a tunable refractive or diffractive SSU, like a liquid crystal modulator or MEMS based rotating prism and/or array of prisms. The IMS may be used as an adaptive device capable of adjusting its spectral and spatial resolution in real-time.

[0072] An IMFU may be fabricated using any available method including, for example, precision diamond raster flycutting, diamond turning using slow slide servo, diamond turning using fast tool servo, micro-diamond milling, precision ruling, CNC based micro-grinding and polishing, grayscale lithography based on direct beam writing, grayscale lithography using masks, multistep reflow lithography. Diamond machining approaches may have several advantages over the other technologies. First, the size, angle, and relative position of each optical component may be held very accurately, since it is determined by precision numerically controlled stages. Second, complex mapping tilt geometries (including roll-yaw-pitch) may be possible with the addition of a precision tilt stage to the diamond turning lathe. Third, the initial prototype development cost and time may be less demanding. And fourth, precision alignment features may be incorporated into the IMFU, thereby increasing the alignment precision of the IMFU with other components, such as baffles and lens focusing arrays.

[0073] In particular, an IMFU may be fabricated using diamond raster fly cutting, which is an appealing diamond machining method for creating thin, straight, high aspect ratio features, such as mirror facets, for the IMFU. As should be understood by one of ordinary skill in the art with the benefit of this disclosure, the aspect ratio of an image is its width divided by its height. In diamond raster fly cutting, a tool may rotate about a spindle and scoops material

out of a workpiece (i.e. IMFU), as illustrated in Figure 4(a). For this example, the workpiece may traverse the y-axis to create a thin mirror facet. To create adjacent facets, the workpiece may step over along the z-axis, as shown in Figure 4(b). This may be repeated down the length of the IMFU until the entire surface is cut. Figure 4(b) illustrates a close up of the tool cutting the workpiece. Note that the different facet angles may correspond to height variations in the workpiece at a specific x-z plane. An example of an IMFU fabricated using diamond raster flycutting is shown in Figures 5(a) and 5(c). In some embodiments, a novel technique may be applied utilizing surface shaped diamond tools to create the individual facet's cross section profile in the IMFU substrate. In traditional raster flycutting, the individual optical components comprising the entire mapper may be created by passing a diamond tool across the mapper substrate material in both lateral (parallel to mapper surface) and axial (perpendicular to mapper surface) directions. With each pass of the tool, a small fraction of the required material may be removed. Consequently, multiple passes may be required to fabricate each optical component, which leads to an expensive and time consuming process. Fabrication with surface shaped diamond tools, on the other hand, may eliminate the need for these lateral translations, requiring only axial passes to create the individual (or group) of optical components.

[0074] Moreover, compact, higher sampling (>100 elements) IMFUs may require much smaller mirror facets. By scaling down the width of the facets, tools that are pre-shaped for the cross section profile of the optical component may be used. This may have several advantages, including a significant reduction in fabrication time, program simplicity, more densely packed mirror facets, and high relative geometric accuracy independent of machine precision for axes perpendicular to the cutting direction.

[0075] The disadvantage of this approach is that there may be little ability to correct for errors in the cross section of the mirror facet due to the tool shape, chips, and/or other defects. This may make the quality of the diamond tools a critical component in the fabrication process. An example of a surface shaped fabrication tool is shown in Figures 4(b) and 4(d). In addition to the tool shown, more complex geometries with multiple facets and/or features are also possible and, in some cases, advantageous to a single surface shaped tool. Figure 5 illustrates an example of a surface shaped tool with 6 facets integrated into the surface. This method may be advantageous for fabrication of complex IMFUs as it (1) decreases the fabrication time, (2) allows for multi-axis tilts, (3) enables densely packed features, and (4) is independent of the precision of the diamond machine for the axis parallel to the cutting direction.

[0076] There are several design parameters that may be considered for the surface shaped diamond tools, such as: included angle θ , primary side clearance angle α , primary tip clearance angle ϕ , top rake angle β , tool width, maximum depth of cut, edge quality, and material. These geometric parameters are illustrated in Figure 4(b) and 4(d). The flat bottom tool tip width and the maximum depth of cut may be the key design parameters of the tool, as they are determinative of the optical design of the system. The tool tip width becomes the width of the mirror facet, while the maximum depth of cut determines the largest achievable y-axis tilt. Proper selection of the other tool parameters may be critical for optimum cutting performance, durability, tool manufacturability, and overall cost.

[0077] The geometry of the IMFU is also an important aspect in the fabrication process. To reduce the effects of edge eating caused by the diamond tool geometry (included angle) shown in Figure 6, the optical components may be (1) staggered in the y-axis, as shown in Figures 7(a) and 7(b), to minimize the step height difference at the edges, (2) grouped in the x-tilts, as shown in Figures 7(c) and 7(d), which decreases the number of facets that have a step height difference, and/or (3) orientated in concave x-tilt facet positions, as shown in Figure 7(e), which reduces the included angle by the magnitude of the adjacent facet tilt.

[0078] Diffraction effects may be another important aspect of the IMFU design, especially for large format spatial imaging situations, which typically require hundreds to millions of miniature optical components tightly packed together. The most dominate diffraction effect is thought to be caused by the width of the facets, which are on the order of 10's – 100's of microns. In the pupil, this diffraction effect may stretch the geometric diameter in the axis conjugate to the width of the facet, as shown in Figure 8(a), creating an elliptical pupil. This diffraction induced elliptical pupil has a two fold effect on the system. First, it may lead to crosstalk. Crosstalk generally refers to the phenomenon that occurs when light from one sub-image from the IMFU enters into the optical path of another sub-image. The IMFU optical component group creating the first sub-image may be adjacent to the optical component group creating the second sub-image. Crosstalk typically occurs at adjacent pupils, collective objectives, and/or re-imaging lenses and often leads to degradation of the final image. For ~1% crosstalk, the minimum separation tilt angle should be approximately $\alpha_{1\%} = \frac{x}{f} \sim \frac{1.35\lambda}{b}$, where

λ , is the wavelength of light, and b is the width of the facet. This crosstalk may be verified theoretically, as shown in Figure 8(b). Note that the pupil distance can change depending on other factors associated with the IMFU, such as facet cross section, surface roughness, and the

incident diffraction limited spot size to name a few. The pupil spacing is typically, but not always, related to the spacing of the collecting objectives and/or the re-imaging lenses of the Selective Imager, as it is often axially symmetric with at least one of the Selective Imager elements. Second, the elliptical pupil may create a “super resolution” effect in the spectral domain. As used herein, “super resolution” generally refers to situations where it is possible to distinguish an image of one point source from an adjacent one closer than the Rayleigh criterion. It should be understood that the Rayleigh criterion is the generally accepted criterion for the minimum resolvable features where the first diffraction minimum of an image of one point source coincides with the maximum of an adjacent point.

[0079] For large format IMS systems, it is often important to maintain optics limited, or close-to optics limited, imaging resolution. For Nyquist sampling, which is the generally accepted minimum resolvable criteria, at least two IMFU optical components must reside within the incident diffraction limited spot to be able to resolve it. Therefore, the individual optical components for the IMFU may range in width from approximately half the width of the incident diffraction limited spot size to a few spot sizes. The diffraction limited spot size may be commonly referred to as the aberration-free image of an infinitesimal point from the optical sample.

[0080] An elliptical pupil may create an asymmetric point spread function with a narrower axis in the spectral direction perpendicular to the spatial direction. This effect may be seen in Figure 9 for an IMFU with 285 facets that are 70 microns wide. The facets are arranged for 25 multi-axis tilts (5 x-tilts, 5 y-tilts). Figure 9(a) shows the raw image of an actual pupil array. For comparison purposes, a theoretical pupil array image is shown in Figure 9(b). Cross section profiles in both the y- and x-axis for both images are compared in Figure 9(c) and 9(d), respectively. For the y-axis (Figure 9(c)), the theoretical and measured pupil diameters and positions may have excellent agreement. However, in the x-axis (Figure 9(d)), the measured pupil diameters may be much larger than expected based on the simulation due to additional optical power for each mirror facet in the IMFU. This leads to the second method to increase the spectral resolution of the IMS system.

[0081] To enhance the spectral resolution of the IMS, the IMFU individual optical components may have optical power for compressing the reflected mapping line widths smaller than the actual components themselves. Alternatively, a separate array of optical components may be added before or after the IMFU to create this optical power. This optical power may be used to narrow the width of the mapping line smaller than the actual IMFU

component, creating additional optical space between adjacent mapping lines for added spectral spread, thereby increasing the spectral resolution of the system. In addition, IMFU optical power may be used to re-image the entrance pupil from the relay optics to the entrance pupil of a Selective Imager collecting objective or array of collecting objectives, creating a more compact and optically efficient IMS design.

[0082] The SSU generally is responsible for the spectral separation of the optical sample. It may be composed of either a refractive, diffractive, or combination optical components. Examples of such components may include wedges, prisms, diffraction grating, grisms (a combination of a prism and grating arranged to keep light at a chosen central wavelength undeviated as it passes through a camera), computed generated holograms, and the like. The SSU may be located in any optical space after the IMFU, although it is preferable to be located at the pupil position of the Selective Imager because, among other things, light from all field points will illuminate the same region of the component providing more uniform chromatic separation. The dispersion direction, or directions, may be in any orientation except for the primary mapping axis of the image mapping field unit. If dispersion takes place in the mapping axis, then the chromatic and spatial information may be lost or diminished. The SSU may be composed of either one continuous optical component over the entire pupil space or an array of smaller optical components. Different SSU designs might be as simple as an optical component giving spectral separation identical for each object point or differentiate between these points. They can be designed as a single SSU optical component or an array of such optical components. Both passive and active components are possible. Active components might be built using liquid crystal modulators (tunable prisms, wedges, diffraction grating, computer-generated holograms ("CGHs"), arrays of wedges having adjustable tilts and wedge angles (possibly MEMS based), electro-optical modulators, magneto-optical components, or a combination of gratings giving different grating constants with changing mutual grating angles. It also may be advantageous to design active or passive prisms with either uniform dispersion and/or zero displacement like that used in direct vision prisms (i.e. Amici type), as this may allow for a more compact, evenly sampled spectral design.

[0083] The Selective Imager works in combination with the IMFU and SSU to rearrange and reimage the dispersed object onto the Image Sensor. As mentioned above, the optical sample may be reorganized spatially and spectrally by the IMFU and SSU, respectively. IMS configurations may include a number of possible Selective Imager types and positions, including (a) optical systems to selectively separate each sub-image, (b) optical systems to

selectively separate each tilt direction, and (c) mixed designs having a number of imagers between the total number of mapping angles.

[0084] Some embodiments provide IMS configurations having an array of Selective Imager re-imaging optical systems to match the same number of optical component groups and/or mapping tilt directions from the IMFU geometry. The advantage of this solution is flexibility of providing various spacing between object zones, but it also may be complex in design and possibly require anamorphic optics for asymmetric mapping geometries. Such methods may be best suited for certain mapper geometries, such as those presented in Figure 3(c) and 3(d), as well as for tunable/dynamic IMS embodiments. Examples of fabricated Selective Imager re-imaging lens arrays are shown in Figure 10. The lens arrays may be composed of a single achromatized doublet lens or several lenses, such as that shown in Figures 10 (b) and 10 (c). The Selective Imager may be corrected for chromatic aberrations, as shown in Figure 11, with spot diagrams and modulation transfer function plots for the F (~486 nm), d (~587.6 nm), and C (~656.3 nm) bands. The design may be diffraction limited at these visible wavelengths. The spectral spread introduced by the SSU unit is around 800 microns, as shown in Figure 12, for various field positions. Mapping aberrations due to distortion also may be minimized, however, since the image may be remapped for display purposes. This may not be of critical importance. For alignment purposes, each sub system may have adjustable focus, either static or dynamic. Possible dynamic optical components may include, for example, MEMS, electro-wetted, micro-fluidic, and liquid crystal lenses, to name a few.

[0085] Other embodiments may provide IMS configurations having an array of optical systems, wherein the number of mapping angles may correspond to the number of required separation pixels for the spectral spread, as illustrated in Figure 13. Note, however, that this correlation is not necessarily one-to-one, as the spectral spread may be tilted to cover more pixels than the number of mapping angles, but it should still be a linear relationship. The mapping optical components may be repeated down the IMFU until the entire image is covered. In Figure 13, for example, there are 9 unique tilt angles that are then repeated down the y axis.

[0086] The magnitude and direction of the IMFU mirror tilt angles may determine where the light from each image mapping line will be directed in the stop, and likewise the intermediate pupil. The number of different mirror tilt angles may be directly proportional to the number of pupil sub regions. In the example shown in Figure 13, there are 9 tilt angles and, therefore, 9 pupil sub regions. Behind these sub regions may be an array of optical systems that re-image the light from each tilt mirror pupil sub region onto an Image

Sensor (CCD or other array detector). Each lens may have a field of view ("FOV") of the entire optical sample but may only receive light from a particular mapping angle. Consequently, there may be a large dark region separating the image mapping lines (or, for more complex mappings, separating mapping line portions or mapping pixels). A SSU may be placed at the intermediate pupil position to disperse the light from each image mapping region or mapping line into an angle that will correspond to these dark regions. The final image on the Image Sensor may look similar to the diagram in Figure 13(c).

[0087] A simple software algorithm may re-map the optical sample as well as the spectral information for each object mapping pixel. Re-mapping might also be performed in hardware, for example using a digital signal processing ("DSP") unit. Both software and hardware solutions may allow real time display of the 3D (x, y, λ) datacube on a monitor screen. In some embodiments, it may be possible for the Image Sensor to comprise multiple detectors corresponding to one or more mapping angles, instead of a single, large format detector. Thus, using Figure 13 as an example, a large format camera, or 9 low resolution cameras, or any number between assuring that all mapping angles are imaged, may be used. Using multiple cameras may be implemented to increase spatial and spectral resolution, minimize unused areas between images, or in applications like infrared ("IR") where large format detectors are generally very expensive or not readily available. A single component Image Sensor may make the system more compact, provide a more uniform response, and simplify the image acquisition.

[0088] In certain embodiments, the IMS may comprise a single tilt axis IMFU. This may be useful to, among other things, decrease the total number of components in the Selective Imager and limit the number of mapping angles, while still providing sufficient separation for spectral spread. For example, the IMFU may only require a few tilts in one direction (around y axis) and, using a slit or pinhole mask in an intermediate image plane, may achieve more separation at the Image Sensor. In other embodiments, increased separation may be achieved by using arrays of spherical or cylindrical reimaging systems. Systems utilizing the arrays of lenses may require an asymmetric shape which may result in an asymmetric point spread function. To compensate, these systems may require an anamorphic relay imaging system. An example of such a unidirectional tilt mapper is shown in Figure 14.

[0089] As mentioned above, the IMS may be reflective. Examples of reflective IMS systems are presented in Figure 15 through 17. Figure 15 illustrates a reflective system with tilted annular mirror. Figure 16 shows a reflective IMS with beam splitter, and in Figure 17, a reflective IMS with a tilted IMFU is shown. In these systems, any choice of SSU as

described above may be used. In addition, the Selective Imager might have many different configurations, for example, consisting of a single collimating objective and array of re-imaging objectives or an array of collimators with an array of re-imaging objectives. The number of array components may also change depending on the design approach and selected critical component configurations.

[0090] One specific example IMS configuration of the present disclosure is a reflective system with annular mirror. This embodiment of the IMS generally maintains high optical throughput with a reflective image mapping field unit. This may be accomplished by placing an annular fold mirror at the stop position between objective 1 and the collecting objective (see Figure 15). Light rays from the optical sample (located at the field stop) may be imaged by objective 1, passing unobscured through a small, central opening in the annular mirror that serves as the stop for that objective. These light rays (depicted by black lines) may be imaged onto the IMFU by the collecting objective. The image may be "mapped" into horizontal sub mapping regions by tilted rectangular mirrors, for example, as illustrated in Figure 13. Each mirror may be the entire length of the image but only one mapping pixel in width. The different mirror angles may be repeated down the IMFU until the entire image is covered. In Figure 13, there are 9 unique tilt angles that are then repeated down the y axis. Light reflected from these mirrors (depicted by colored lines in Figure 15) may travel back through the collecting objective, but to the annular mirror region outside of the first objective's stop. The annular mirror surface may act as the stop for the collecting objective (L2), and may reflect light out of the path of the original system toward a pupil relay. Note that the collecting objective and re-imaging lens array form the Selective Imager.

[0091] The pupil relay placed between the collecting objective and the re-imaging lens array may image the annular mirror (stop) to a more accessible intermediate pupil location while adding the appropriate magnification for fitting the final image onto an Image Sensor. The magnitude and direction of the mapping mirror tilt angles may determine where the light from corresponding image mapping line will be directed in the stop or its conjugate intermediate pupil location. The number of different mapping angles may be directly proportional to the number of pupil sub regions. An array of lenses may re-image the light from each sub-pupil of a particular mapping sub region onto an Image Sensor, such as a CCD detector or other array detectors. Each lens may have a FOV of the entire optical sample, but each may only receive light from a particular mapping angle. A SSU may be placed at the Selective Imager stop or its conjugate

pupil position to disperse the light from each mapping line or mapping region into an angle that will correspond to these dark regions.

[0092] This above described system may have the following slight modifications while still maintaining its overall functionality. The annular mirror may be faceted to deviate some of the mapped light into different directions out of the path of the original system. The annular mirror may have the unobscured region located at any position on the surface although the central region is preferable. The mirror surface does not have to be flat, but may have some optical power associated with it. The collecting objective may be arrayed to accept unique (or a few) mapping angles. The pupil relay also may be arrayed and/or made anamorphic for compression of the spatial data. The SSU also may be a single or array of systems. The SSU may be a refractive, diffractive, and/or combination component. The lens array may be made anamorphic. The annular mirror may have the SSU placed on its surface or close to the surface.

[0093] Another specific example of an IMS configuration of the present disclosure is a reflective IMS with beam splitter. This reflective IMS with beam splitter may consist of two optical paths connected by a beam splitter. One is called the “re-imaging” optical path (composed of L0, L1, L2, L3, and IMFU), and the other is called the “mapping” optical path (composed of IMFU, L3, L2, L4, array of L5 optical systems, SSU, and Image Sensor). One embodiment of the system is depicted in Figure 16. Therein, the IMFU reflects light into $N = 25$ different pupils, but any number can be used. The size of the void region on the Image Sensor may be proportional to N . The apertures of the L0, L3, and L5 array are conjugated by image relay systems. A dispersive prism may be placed at the entrance pupils of the L5 array to spread the spectrum from the mapping line from the optical sample, thereby functioning as the SSU. After passing through L3, L2, L4, and L5, the image of the optical sample may be mapped; the beams may be collimated, dispersed, and re-imaged. In effect, an image may be mapped onto the Image Sensor in a pattern of mapping lines dispersed over the detector area. Each x , y , and λ component may be directly mapped to a different camera pixel. The imaging system may be telecentric in both object space and image space, providing lower sensitivity to defocus. Unfortunately, this setup may be quite energy inefficient, and it may lose up to about 75% of light (due to two passes at a 50% beam splitter). Its biggest advantage may be simplicity and symmetry, which may allow an easy use of entire Image Sensor array.

[0094] Another specific example of an IMS of the present disclosure is a Reflective and Tilted IMS. One such IMS system is illustrated in Figure 17, consisting of optional relay lens, the IMFU, array of collimating lenses, a blazed diffraction grating, array of

re-imaging objectives, and an Image Sensor located in the image plane. Note that the diffraction grating rulings lie parallel to the plane of the page of this document, so the dispersive effect is not seen in the cross-section presented. The IMFU modeled here has four tilted facets (mapping lines) located on different image heights. It may enable re-organization of the image into mapping lines along the x direction separated by multiple mapping pixel rows, as illustrated in Figure 17. The diffraction grating may spread these mapping lines in the y-direction, which may enable both spatial and spectral information to be recorded simultaneously without scanning. One advantage of this system is that it avoids light losses by a beam splitter. Its biggest disadvantage may be a tilt of the mapping component, which may increase result some IMFU regions being out-of-focus. This may be compensated by tilting an object/intermediate image to optimize conjugate planes.

[0095] As mentioned above, the IMS may be refractive. Such IMSs are similar in concept to the reflective systems, except the IMFU may be a refractive component instead of being reflective. One advantage of such IMSs is the fact that the system can remain unfolded, making the opto-mechanics less complicated and more compact. Refraction effects may also introduce some undesired dispersion, creating spectral separation. As should be understood by one of ordinary skill in the art with the benefit of this disclosure, spectral separation during mapping may cause neighboring image point to overlap in the final image, obscuring the information, and requiring image processing correction. This may compromise one of the main advantages of the IMS system: direct unambiguous data acquisition for real-time image display. Therefore, it may be advantageous for the refractive optical components in the IMFU to be corrected for this spectral separation and other chromatic aberrations. This can be done a number of ways, including, but not limited to: combining two or more refractive materials with different dispersion, combining a refractive and reflective component, and combining a diffractive and refractive component. Light from the optical sample may be relayed onto the IMFU by Relay Optics L1 (for example, as illustrated in Figure 18). The image may be “mapped” into many sub regions or individual mapping pixels by tiny prisms. These prisms may have different angles associated with them and may cause the light to travel along different paths, as shown in Figure 18 by the different colors. The different optical paths from the “mapped” image may be collected by Objective L2 and directed to specific sub regions in the pupil. The SSU may disperse the light in these sub regions into different angles that correspond to the dark regions created by the IMFU in the final image. Immediately following the SSU, an array of lenses may re-image the light onto an Image Sensor (e.g., CCD, CMOS, or similar

detector), where a simple software algorithm can re-map the optical sample with its spectral information.

[0096] This above described system may have the following slight modifications while still maintaining its overall functionality. Objective 2 may be arrayed to accept unique (or a few) mapping angles. The spectral separation unit also may be a single or array of systems. The spectral separation unit may be a refractive or diffractive component. The lens array may be made anamorphic for spectral or spatial information compression.

[0097] Another approach to certain IMSs of the present disclosure is based on the application of an “array of lenses” located such that the field stop coincides with the focal plane of lenses. Such IMS configurations may use reflective and refractive approaches. The micro lens array may play the role of a parallel sampling probe. Figure 19 illustrates this concept. The overall imaging principle remains the same, and the IMS may be supplemented with other components similar to those used in the layouts presented above. The spatial resolution of the system in this case may be determined by the packing density of lenses in the array, since each lens may be responsible for a single image point. Light rays launched from the field stop may emerge parallel to the optical axis after passing the micro lenses. On reflection at the mapper, the optical rays may propagate into specific directions to achieve the required image mapping. One advantage of this approach is its insensitivity to defocus. The system’s accuracy may rely on the uniformity of lenses in the array and quality of beam collimation.

[0098] To capture a greater quantity and/or quality of spectral information, a dichroic mirror may be added to the image space of the Selective Imager, as shown in Figure 20. The dichroic mirror may enable the system to collect spectral information from the optical sample in two or more distinct spectral bands, including adjacent spectral bands, such as visible and near infrared, and non adjacent spectral bands, such as ultraviolet and midwave infrared. In addition, the spectral information also may be enhanced within a single spectral band, increasing the spectral resolution by two or more times the original system. The configuration illustrated in Figure 20 may utilize an additional camera (Image Sensor detector #2) to collect the second band of information. In this diagram, Image Sensor detector #1 may collect light from the red to green region of the visible band, and Image Sensor detector #2 may collect light from green to UV. However, this concept also may be applied to a single camera Image Sensor in which filters of selected wavelength regions are placed in front of rows of neighboring detector pixels as illustrated in Figure 21. The unfiltered Image Sensor detector may only spread spectrum from one mapping line from the optical sample (line #1) to the next mapping line from the optical

sample (line #2), as shown in Figure 21(a). For this example, there is no room for the Blue-UV spectrum from line #1. By adding filters (for example, see Figure 21(b)) to the Image Sensor and oversampling the point spread function of the image, it may be possible to obtain the additional spectrum from line 2 (for example, see Figure 21(c)). The tradeoff with this approach is that the optical throughput of the system may be decreased. This may be overcome with lens arrays similar to those already used in CCD and CMOS image detector to overcome fill factor issues.

[0099] Another IMS configuration may use micro lens arrays and/or micro field stop arrays to optically compress the facets on the mapper, creating additional space for spectrum. One possible embodiment is illustrated in Figure 22. In this example, a set of micro cylindrical lens arrays are placed near the sub-image plane after the Selective Imager. The lens array and/or micro stop array may add additional optical power in the sagittal plane of the image, but not the meridional plane. This may create an asymmetric point spread function on the final image plane that is narrower in the sagittal plan, which is also the direction used for spectrally spreading the image.

[00100] A dynamic IMS system is presented in Figure 23. This system has the ability to act like a digital and optical zoom camera system for the entire 3D (x, y, λ) datacube, changing IMS configuration during operation to obtain different spatial and spectral sampling from one or multiple mapping regions of the optical sample. It may be possible to zoom into one or more regions of interest ("ROI") and obtained higher spectral and spatial resolution. As used herein, "zoom" generally refers to increasing the number of samples over a ROI of an image of the optical sample. Digital zoom may be an electronic reconfiguring of the array of sensors comprising the Image Sensor to change the number of samples in selected regions of the Image Sensor. Optical zoom generally means hardware reconfigurations, whereby the image of the optical sample is altered to change its sampling by the Image Sensor. Spectral zoom generally means increasing the number of sensing elements over a given spectral range, or decreasing the spectral range over a given number of sensing elements. Spatial zoom generally means increasing the number of sensing elements over a given spatial mapping region, or decreasing the spatial mapping region over a given number of sensing elements. This may be accomplished by utilizing dynamic components for one or more of the critical components of the system: IMFU, SSU, Selective Imager, and, optionally, the image relay lens. The relay lens may change the size of an image of the optical sample, increasing the image sampling on the IMFU, and thereby zooming the spatial domain. If multiple IMFUs and/or dynamic relay lenses are used, similar to

Figure 25, it may be possible to provide optical zoom to for more than one location on the image. The dynamic IMFU may use MEMS techniques to adjust mirror tilts to selectively reflect image mapping pixels of interests toward the Selective Imager, creating zoom in spectral and spatial domain. These mapping pixels may then be spectral spread more or less by dynamically
5 adjusting the dispersion of the SSU. One possible approach for adjusting the spectral spread of the SSU is to use a plano-convex and plano-concave lens pair or similar materials to create a prism like structure (for example, see Figure 23). By rotating the plano-convex lens, the angle of the prism may change, causing the dispersion of the prism to change as well. The last component that can dynamically change is the lens array in the Selective Imager. By adjusting
10 the power of the lens array, the final image size also may scale, creating increased sampling of the image both spectrally and spatially. This may also make it possible to image faster (by binning the camera) and/or improve dynamic range.

[00101] As an alternative to the previously mentioned refractive or reflective approaches, the IMS system may use a waveguide mapper to create an optically void region
15 between adjacent image points, as shown in Figure 24(a). The relay optics (primary pupil and zero, one, or more optional relay lenses) image the optical sample onto the input face of the waveguide mapper. As shown in Figure 24(b), the waveguide mapper may guide light from each individual waveguide to an isolated mapping pixel at the output of the mapper face. Note that this mapping may be coherent or incoherent between the mapper input end and output end. The
20 mapper face may be imaged by a large FOV objective (L2), dispersed by the SSU, and imaged by the re-imaging lens onto an Image Sensor, such as a CCD detector. This configuration may utilize a less complicated Selective Imager than the refractive and reflection components, however, it may have lower optical throughput due to the cladding around each waveguide structure.

[00102] Another embodiment of an IMS system includes two or more IMFU
25 elements that are imaged onto each other. In other words, they are image conjugates of each other. This multiple IMFU conjugate configuration is shown in Figure 25. In this design, the optical sample may be imaged on the first IMFU through the optional relay lenses. This relay system is optional, as the optical sample may be imaged directly onto the first IMFU with any
30 fore optics. The first IMFU may be imaged onto the second IMFU by the IMFU relay lens. There may be multiple IMFU relay lens and multiple IMFUs, either sequentially cascaded one after another or in parallel, forming an array of IMFUs and relay lenses. The array approach may be beneficial for keeping the system compact. For Figure 25, only two IMFUs are shown

for simplicity, not limitation of the design concept. After the last IMFU (the second IMFU in Figure 25) and Selective Imager, the SSU and Image Sensor function in a similar way as the prior concepts for example Figure 18. The IMFUs in this design may be either static or dynamic or a combination. This type of IMS system may be advantageous in dynamic systems (Figure 5 23), allowing for the first component to select one or more ROIs from the optical sample, and direct these ROIs to the second IMFU for higher sampling and mapping to one or more Image Sensor detectors. This approach also may be capable of simplifying the design of each IMFU with each conjugate IMFU responsible for only one aspect of the final mapping. For instance, the first IMFU may be responsible for tilts in the x-axis, while the second IMFU may be 10 responsible for tilts in the y-axis. This implies that each IMFU for this embodiment does not have to have the same geometry or function as the other IMFUs, and each IMFU may act independently or dependently.

[00103] As mentioned earlier, the IMS may be adapted for many various applications. For example, the IMS may be particularly well suited for endoscopy. An 15 endoscope version of the IMS concept is illustrated in Figure 26. Discussion of the IMS system operation begins at the tissue (distal) side of the coherent multi-fiber bundle ("MFB"), where a broadband source may illuminates an area of the tissue (either macroscopic or microscopic in size) which becomes our optical sample. Other endoscopic imaging components also may be used in substitution or addition to the MFB presented in Figure 26. These endoscopic imaging 20 components may include: incoherent fiber bundle, miniature objective, miniature lenses and grin lenses. Reflected and/or fluorescent light from the tissue may be collected and imaged through a miniature objective onto the MFB distal tip and then transferred to the proximal end. The image relay system may magnify and re-image the tissue image from the MFB proximal face onto the IMFU. For this illustration, the IMFU may be composed of an array of mirror facets with 25 dimensions that correspond to 1 x 200 mapping pixels at the image plane. Note that the IMFU also may be composed of an array of prisms, lenses, and/or a combination of components. Each mirror facet may deviate a portion of the tissue image (optical sample) to a particular region in the pupil of the Selective Imager (shown by different ray colors). The light may be spectrally separated (i.e. dispersed) in the pupil by a SSU (i.e. prism array) into a range of angles in a plane 30 different in direction than the mapping plane. A re-imaging lens array may image each sub-region onto an Image Sensor. Each sub-image may contain spatial and spectral information for a set of mapping regions. Finally, through simple software remapping, the sub images may be recombined to form an "unmapped" image of the optical sample (tissue) while preserving the

spectral signature for each mapping region. Since there is no scanning or image processing, the system may acquire and display hyper-spectral images in real time which is important for endoscopy applications.

[00104] Ophthalmologists have long relied on optical devices for evaluation of various eye conditions and diseases. Of particular importance is imaging the retina of the eye, which is located at the back inner surface of the eye and contains the light sensitive photoreceptors for converting the optical signals to signals that can be processed by the brain. Retinal observation and image capture requires the use of a complex optical device, called a Fundus camera, which is capable of illuminating and imaging the retina simultaneously. There are two main types of Fundus camera designs that vary based on the illumination system, either external or internal illumination. The incident illumination provided by either type is scattered by the retina and then captured by the imager portion of the Fundus camera where it can be viewed by the ophthalmologist directly and/or captured by an image sensing device. Ophthalmologists are increasingly using digital detectors such as CCD or CMOS cameras to record a picture of the retina. These digital pictures can be used to identify certain illnesses as well as track their development over the lifetime of the patient. In this context, an IMS system may become an important imaging tool for ophthalmology, where it can obtain a 3D (x, y, λ) image of the retina with additional diagnostic information contained in the spectrum from each mapping pixel within the image. Figure 27 shows an example of an IMS system that is incorporated into a Fundus camera. The IMS system is positioned at the sideport or camera port of the Fundus camera where an image of the retina is located. The IMS system also may be used as a standalone system for imaging the eye. For a standalone IMS system, the illumination may be integrated into the IMS system, either external or internal to the system in a similar fashion to that commonly used in Fundus cameras. The main advantage of an IMS system for ophthalmic applications is that the IMS system may collect its 3D datacube in a true parallel fashion for quick real-time imaging. This may be important for mitigating any temporal ambiguities due to involuntary eye movements. The parallel acquisition may also decrease the intensity of illumination, since the collected signal from every image point is integrated at the same time, making it is less irritating for the patient's eye. The simple software image remapping needed for the IMS system may also allow for real-time feedback for the ophthalmologist, helping to direct the examination and provide better quality diagnostic information.

[00105] To facilitate a better understanding of the present invention, the following examples of specific embodiments are given. In no way should the following examples be read to limit or define the entire scope of the invention.

EXAMPLES

5 [00106] A working bench top prototype IMS and prototype of a mapping element (or mapper, Image Mapping Field Unit, or “IMFU”) were assembled, configured as a reflective Image Mapping Spectrometer (“IMS”) with beam splitter. A schematic of the prototype system and a picture of the actual setup are presented in Figure 28.

10 [00107] The optical sample for this IMS configuration came from an inverted microscope, namely, an Axio Observer A1 or AX10, commercially available from Carl Zeiss, Inc. For demonstration purposes, the Selective Imager lens array was replaced with a single lens (low magnification microscope objective) and was moved to different pupil locations to image the corresponding tilt angle field of views (“FOVs”). The IMFU prototype was fabricated using raster fly cutting in high purity aluminum. The mapping element had 5 tilt angles in one
15 direction only (175 ramp mirrors total). To fabricate the IMFU, a Nanotech 250 UPL Diamond Turning Lathe was used. The cutting process was lengthy for the first optical component, as it took about 120 hours. Once the desired mapping element has been made, it may be mass produced either by replication or molding processes (e.g., injection molding, stamp molding, etc.) to make it more affordable.

20 [00108] Figure 29(a) shows the first prototype IMFU. The individual optical component facets have further been characterized to verify angles and surface quality using a white light interferometer, a NewView 5000, commercially available from Zygo Corporation, as shown in Figure 29(c). Baffles may be added in front and to the sides of the mapping element to reduce scattered light from the transitions mapping optical components. Lens arrays may also be
25 added to the mapper to help reduce scattered light by focusing it away from the edges of the mapper’s optical component and more to the center of the surface of mapping optical components. Lens arrays also may reduce the effects of neighboring IMFU optical component shadowing. This is especially important at the edges of the optical components, where the height differences may be the largest. Although the prototype IMFU was made using diamond fly
30 cutting technology, it also may be produced using other technologies, like diamond milling and grayscale lithography, depending on the desired geometry. Grayscale lithography is an alternative technology for mass producing this element, but it may require significant process development time and cost in the initial development stage.

[00109] Figure 30 shows initial imaging experiments performed with the system prototype. Figure 30(a) shows an image of a 1951 USAF resolution test target for the central FOV. Only one mapping direction is demonstrated in the figure and no dispersion was introduced in this case. Figure 30(b) shows an image of the Selective Imager pupil when the
5 IMS is imaging the output from a single mode ($\lambda \sim 630\text{nm}$) fiber laser (object) onto at least five mapping lines of the image mapper. In this example, each mapping line of the IMFU is generally a miniature ramp mirror that may be able to reflect a single (possibly discontinuous) line of the incident image into a unique direction. The five bright regions correspond to light from the object reflected from the different line optical components and their corresponding
10 angles. Diffraction and stray light effects caused by the linear IMFU geometry and surface roughness account for the light intensity outside of these central regions. When the re-imaging lens is moved from one pupil position to the next, the resulting image is similar to the one shown in Figure 30(a) but for a different set of linear mappings.

[00110] Figure 30(c) presents an image taken with the prototype system (minus the
15 IMFU and the SSU) of a fiber optic illuminated with a halogen light source. This polychromatic image is composed of a broad spectral band and represents a typical image one would obtain from a standard imaging system. This image typically would appear as a white circle, and all of the spectral information would be lost. In this image, there are some blue and red outer bands in the image due to lateral chromatic aberrations which may be corrected in the final system. When
20 the prototype system is reconfigured to include IMFU and the SSU, the full spectral signature of this polychromatic image may be obtained. This is illustrated in Figure 30(d) for a set of ramp mirrors with identical tilt angles. As one can see with the spectral data for the image, mapping lines may be dispersed into the void regions between the neighboring mirrors – mapping components (repeated red to green regions). To reconstruct the final image, the re-imaging lens
25 may be translated to the other pupil positions to capture images of the other mapping lines, and simple image processing may be done to reconstruct the original image with its spectral signature.

[00111] A second working prototype IMS was constructed to demonstrate its ability to obtain fluorescence microscope images. The IMS could obtain a 3D (x, y, λ) datacube
30 of $100 \times 100 \times 25$ sampling, which corresponds to about 0.45 microns and about 5.6 nm resolution in spatial and spectral domains respectively. The IMS system was coupled to an AX10 inverted microscope, commercially available from Carl Zeiss, Inc., as the fore optics. A photograph of the prototype system is shown in Figure 31(a), and the schematic layout is

presented in Figure 31(b). Specimens were placed on the microscope stage and illuminated by a 120W X-cite[®] arc lamp, commercially available from EXFO Life Sciences & Industrial Division. The fluorescent signal was collected by an EC Plan-Neofluar, commercially available from Carl Zeiss, Inc., $40\times$ /N.A. ~ 0.75 objective. The intermediate image was formed outside
5 of the microscope side image port, co-located at the field stop of the IMS system. The intermediate image at the field stop was first re-imaged by an about $10\times$ magnification image relay system (telecentric both in object and image space) onto a custom-fabricated image IMFU. One role of this image relay system is to preserve the image resolution by matching the size of image PSF with that of IMFU. The other is to provide strict telecentricity at the side of IMFU,
10 which provides correct guidance of chief rays. The IMFU was a one-dimensional mirror array that had 25 different two-dimensional tilt angles (0° , $\pm 0.23^\circ$, $\pm 0.46^\circ$ with respect to both x and y-axes), and which could reflect zones of mapped image into 25 different directions. The total number of mapping optical components on the IMFU was 100, and each one had dimensions of about $16\text{ mm} \times \text{about } 160\text{ }\mu\text{m}$ in length and width respectively. In Figure 31(b), only tilt angles
15 with respect to the y-axis are shown. The redirected light was gathered by the collecting lens (about 130 mm Tube lens, commercially available from Carl Zeiss, Inc., N.A. ~ 0.033 , FOV $\sim 25\text{ mm}$), and formed 25 separate pupils at the pupil plane. An about $5.56\times$ beam expander, commercially available from Edmund Optics (Gold Series Telecentric Lenses 58258, FOV $\sim 8\text{ mm}$), adjusted the pupil dimensions to match those of the re-imaging lens array optics. The
20 magnified pupils were dispersed by a custom prism, SF4, about 10° wedge angle, commercially made by Tower Optics, and re-imaged onto a large format CCD camera (Apogee U16M, 4096×4096 pixels, about 9 microns pixel size, RMS noise: 10.5 e-, Dark current: 0.13 e-/pixels) by a 5×5 array of reimaging systems. Each re-imaging lens was composed of an about 60 mm F.L. positive achromatic doublet (Edmund Optics 47698, dia $\sim 6.25\text{ mm}$) and an about 12.5 mm F.L.
25 negative achromatic doublet (Edmund Optics 45420, dia $\sim 6.25\text{ mm}$) to form a long focal length lens (F.L. $\sim 350\text{ mm}$). Note that the IMS prototype presented here does not use the full CCD resolution. However, this large Image Sensor may allow improved resolution of the system resolution in future system development.

[00112] The format of the final image may be very important for maximizing the
30 mapping of the 3D (x, y, λ) datacube onto the recording 2D Image Sensor. In many cases, it is advantageous for each detector, or pixel, on the Image Sensor to record a signal from the optical sample. For unambiguous data collection, each voxel in the datacube may correspond to about one pixel on the Image Sensor. Unambiguous mapping that efficiently utilizes all of, or a large

number of, the available detectors in the Image Sensor may require the sub-images from the IMFU to be in close proximity to each other. Note that in the majority of configurations, the Image Sensor may have more than one sub-image of the IMFU. To correct for fabrication errors, optical aberrations, stray light, other unaccounted for fabrication errors, and optical effects, the IMFU geometry may provide for some distance between adjacent sub-images. Ideally, this unused Image Sensor surface area should be no greater than about 40% of the total detecting surface area. On the other hand, it may also be beneficial for the sub-images to overlap to include both ambiguous and unambiguous data, which may improve the available spectral and spatial content of the system. This overlap may be as small as a few detectors on the Image Sensor, and may range up to every detector on the Image Sensor. As previously mentioned, the disadvantage of too much sub-image overlap is that software reconstruction algorithms may become quite time consuming, eliminating the ability of the IMS to display data in real-time. It also may be advantageous for the sub-images of the final mapped image to be arranged to match industry standard camera formats and aspect ratios like those listed in Table 1, although custom formats also may be used.

Table 1: Image sensor formats

Imager Format	Aspect Ratio	Width (mm)	Height (mm)	Diagonal (mm)
¼ in.	4:3	3.2	2.4	4
1/3 in.	4:3	4.8	3.6	6
½ in.	4:3	6.4	4.8	8
2/3 in.	4:3	8.8	6.6	11
1 in.	4:3	12.8	9.6	16
4/3 in.	4:3	17.8	13.4	22.3
APS	3:2	25.1	16.7	30.1
35 mm	3:2	36.0	24.0	43.3
48 x 36 mm	4:3	48.0	36.0	60.0
645	4:3	56.0	41.5	69.7
10.5 / 16.8 MP	1:1	36.8	36.8	52.1
4.3 MP	1:1	50.02	50.02	70.7

[00113] The listed dimensions in Table 1 are approximate, as each Image Sensor manufacturer varies slightly. Some of the most common aspect ratios may be 1:1, 3:2, and 4:3

[00114] The FOV of the reimaging lens set in this prototype IMS was designed to be overlapped with adjacent lens sets to maximize the usable area of the CCD camera. As the whole IMFU plate's image had a square shape, while the FOV of the reimaging lens set was circular, four void regions outside the IMFU plate's image but inside the FOV existed (see Figure 32). Because of these void regions, the FOV of neighboring reimaging lens sets were allowed to overlap. This allowed a fully utilized imaging area on the CCD camera. The CCD camera used a 10.5 / 16.8 MP format chip comprising 16 megapixels within a square (36.8 x 36.8 mm) surface area.

[00115] To verify the image performance and test the spatial and spectral resolution of the IMS prototype, an undispersed 1951 USAF resolution test target was imaged, and the point spread function ("PSF") of a single image mapping line (from single mirror mapping component) was measured. Spectra images of test samples made with fluorescent beads were obtained. The results are shown in Figures 33-36.

[00116] A third prototype IMS was constructed to demonstrate a large format configuration capable of collecting a 3D (x, y, λ) datacube of 285 X 285 X 62 for fluorescence specimens. The layout of the IMS configuration is similar to the 2nd prototype and is shown in Figure 37. This IMS configuration represents major technology advancements in a large format IMFU. The IMFU had densely packed mirror facet optical components that are only about 70 microns wide, enabling 285 facets to reside within the FOV of the relay optics. Due to the small size of the facets, diffraction effects had to be considered in the design, and additional tilt angles were applied to minimize crosstalk between sub-imaging systems. Lastly, the IMFU geometry was optimized to reduce edge eating effects and improve system throughput.

[00117] The biological imaging capability of the third prototype was evaluated by imaging bovine pulmonary artery endothelial cells incubated with MitoTracker Red CMXRos to label the mitochondria, BODIPY FL phalloidin to label the filamentous actin (F-actin), and DAPI to label the nucleus. A reference image taken with a color CCD camera is shown at the top left corner of Figure 38 for comparison purposes. The lower sequence of images was taken with an IMS system in a single, about 4 sec integration event. A sample of 25 spectral images are display over an about 505 to about 684 nm spectral range, with an average sampling of about 5 nm. Spectrally encoded features within the cell are easily identifiable and show a strong correlation with the reference image.

[00118] To manufacture IMFUs with a variety of geometries, three different surface shaped tool designs have been developed. Table 2 lists the different design

specifications for each surface shaped tool. Tool #1 was the first surface shaped tool used to fabricate the 100 component IMFU used in the IMS fluorescence hyperspectral microscope shown in Figure 31. This surface shaped tool has an about 160 micron wide flat bottom tip and was used to create a square shaped IMFU with a side length of about 16 mm. Tool #2, an about 75 micron flat bottom surface shaped tool, was developed for the larger format IMS system, shown in Figure 37, which still resides within the FOV constraint of the collecting objective. This surface shaped tool increases the spatial sampling to a 250 component IMFU. Tool #3 is also about 75 microns wide, but it has a reduced included angle to minimize the effects of edge eating.

Table 2 – Surface Shaped Flat Bottom Tool Design Parameters

Parameter	Tool #1	Tool #2	Tool#3
Included Angle, θ , (deg)	20 $\pm$ 0.5	20 $\pm$ 0.5	5 $\pm$0.5
Side clearance angle, α (deg)	3	3	3
Tip clearance angle, ϕ (deg)	6	5	5
Top rake angle, β (deg)	0	0	0
Tool Tip Width, (μ m)	150 $\pm$ 15	70 $\pm$ 7	70 $\pm$ 7
Max. Depth of Cut, (μ m)	500	300	300
Edge quality	750 X	750 X	750 X
Material (Diamond)	Synthetic	Synthetic	Synthetic

[00119] For fabrication of the IMFUs, a high precision CNC 4-axis diamond lathe (Nanotech 250UPL) was used. This machine has about 200 mm of travel for each axis (x, y, z) with nanometer level precision. The workpiece was mounted on two stages, with y and z axis movement, while the spindle and diamond tool were mounted on the x axis stage see Figure 39(a). The mirror optical component facets were cut by moving the workpiece up and down in the y axis. Tilts in the y direction were achieved by moving in both the x and y directions while cutting each mapping line optical component. After cutting a mapping line optical component, the spindle and tool moves away from the workpiece, rewinds, and begins cutting the next mapping line optical component. The workpiece also steps over in the z axis by the tool width prior to cutting the next mapping line optical component. The x-tilts were obtained by mounting the workpiece to a goniometer (Newport P/N: GON40-U with manual high resolution micrometer P/N: HR-13) with its cutting surface coincident with the goniometers axis of rotation (see Figure 39(b)). Due to the manual rotation of the goniometer, x-tilts were fabricated at the

same time. When finished, the goniometer is adjusted to the next x-tilt, and the process is repeated until all mirror optical component facets are fabricated. Y height compensation factors were applied for the different x-tilts. For large x-tilt angles, z-axis compensation factors also may be used to compensate for the cosine effect.

5 [00120] To manufacture an IMFU optical component, in general, a rough cut is performed initially to get the different mirror facets into the aluminum substrate. The substrate also may be made out of any other diamond machinable material, such as those listed in Table 3. After this step, a fine cutting program is used to clean up the IMFU optical component, producing the best surface roughness and removing cosmetic imperfections, such as metal flaps,
10 chips, and other debris.

Table 3 – Possible IMFU substrate Materials

<u>Metals</u>	<u>Polymers</u>	<u>IR crystals</u>
• Aluminum	• <u>Acetyl</u>	• <u>Cadmium Sulfide</u>
• Alloys	• <u>Acrylic</u>	• <u>Cesium Iodide</u>
• Brass	• <u>Fluoroplastic</u>	• <u>Indium Antimonite</u>
• Copper	• <u>Nylon</u>	• <u>Magnesium Fluoride</u>
• Gold	• <u>Polycarbonate</u>	• <u>Phosphate (KDP)</u>
• Nickel	• <u>Polypropylene</u>	• <u>Tellurium Dioxide</u>
• Silver	• <u>Polysulfone</u>	• <u>Cadmium Telluride</u>
• Tin	• <u>Silicone</u>	• <u>Gallium Arsenide</u>
• Zinc	• <u>Olefin</u>	• <u>Iridium</u>
	• <u>Zeonex (polyolefin)</u>	• <u>Potassium Bromide</u>
		• <u>Silicon</u>
		• <u>Zinc Selenide</u>
		• <u>Calcium Fluoride</u>
		• <u>Germanium</u>
		• <u>Lithium Niobate</u>
		• <u>Potassium Dehydrogenate</u>
		• <u>Sodium Chloride</u>
		• <u>Zinc Sulfide</u>

15 [00121] Figure 40(a) shows a picture of the final large format (250 component) IMFU fabricated using tool #3. Figure 40(b) shows a close up side view of the

IMFU, showing the excellent alignment of the facets. The x-tilt grouping and concave orientation are easily observed as well as the staggered y-tilts.

[00122] The mirror optical component facet tilts and widths were measured using a white light interferometer (Zygo NewView). Before component testing, the IMFU was placed on the interferometer's motorized 4-axis stage (X, Y, θ_x , θ_y) and adjusted to align the reflected light from the zero tilt (x- and y- axis) mirror facet of the IMFU with the optical axis of the system. Any residual tilt was recorded and subtracted from the other facet tilt measurements. A 10X Mirau Objective with a 1.0X field lens (FOV = 0.72 mm x 0.54 mm, Res. = 1.12 microns) was used to collect the data. Ten measurements were taken for each tilt position and averaged together. Table 4 shows the final results, comparing the measured values to the designed tilt values. The results from this study demonstrate an excellent agreement between the desired tilt values and those actually measured. The largest tilt error was -2 mrad for the x-tilt ($\alpha_2=0.010$ rad.), with most of the tilts having no significant error.

Table 4 – Comparison of IMFU tilt designed and measured values

x-tilt (α 's)	y-tilt (β 's)	Ideal (rad.)	<u>Measured</u>		<u>Error</u>	
			(α 's)	(β 's)	(α 's)	(β 's)
α_1	β_1	+0.020	+0.020	+0.020	0	0
α_2	β_2	+0.010	+0.098	+0.010	-0.002	0
α_3	β_3	0	-	-	-	-
α_4	β_4	-0.010	-0.010	-0.010	0	0
α_5	β_5	-0.020	-0.021	-0.020	+0.001	0

15

[00123] The width of each optical component facet was measured by taking a cross section profile across its surface at the left, center, and right edge of the facet. Figure 42 shows typical results obtained from these measurements. During the fabrication process, an approximate 5 micron overlap was introduced to remove a thin metal flap between adjacent facets. This overlap changes the designed width of the facets from about 75 microns to between about 70-65 microns, depending on facet position. For the center x-tilts (2-4) the measured widths were within about +/- 1 micron of the 70 microns; however, for the edge positioned x-tilts (1 & 5) this changes to about 50-70 microns, depending on the y-tilt. The highest mapping line optical component due to the y-tilt will be the thinner due to this overlap as well as some edge eating, as shown in the 2D intensity maps in Figure 41.

25

[00124] The roughness of the mirror optical component facet surfaces reduces the final image contrast and throughput of the IMFU. To quantify this effect, a white light

interferometer with a 50X Mirau Objective, 2.0X field lens (FOV =0.07 mm X 0.05 mm, Res. = 0.11 microns) was used. Figure 42 shows a typical roughness result obtained from a single facet. For this fabrication method, the tool imperfections create lines along the length of the facets. To gain a more statistical estimate of the IMFU's surface roughness, ten randomly selected facet surface regions were measured and found to have an average rms roughness of 5.3 +/-1.2 nm. The optical throughput of the IMFU was estimated to be approximately 97% based on this roughness value.

[00125] Notwithstanding that the numerical ranges and parameters setting forth the broad scope of the invention are approximations, the numerical values set forth in the specific examples are reported as precisely as possible. Any numerical value, however, inherently contain certain errors necessarily resulting from the standard deviation found in their respective testing measurements.

[00126] Therefore, the present invention is well adapted to attain the ends and advantages mentioned as well as those that are inherent therein. While numerous changes may be made by those skilled in the art, such changes are encompassed within the spirit of this invention as illustrated, in part, by the appended claims.

CLAIMS

What is claimed is:

1. An image mapping spectrometer comprising:
an image mapping field unit;
5 a spectral separation unit; and
a selective imager.
2. The image mapping spectrometer of claim 1 further comprising at least one image sensor.
3. The image mapping spectrometer of claim 2, wherein each image sensor
10 comprises an array of quantitative electromagnetic radiation detectors.
4. The image mapping spectrometer of claim 2, wherein each image sensor has an aspect ratio selected from the group consisting of: about 1:1, about 3:2, and about 4:3.
5. The image mapping spectrometer of claim 1 further comprising a relay lens.
6. The image mapping spectrometer of claim 1, wherein the image mapping field
15 unit comprises an array of optical components, and wherein each optical component comprises at least one component selected from a group consisting of: a refractive component, a reflective component, and a waveguide.
7. The image mapping spectrometer of claim 6, wherein each of the optical components has at least one spatial dimension no larger than an incident diffraction limited spot
20 size of the image mapping spectrometer.
8. The image mapping spectrometer of claim 6, wherein at least one optical component comprises a mirror facet tilt.
9. The image mapping spectrometer of claim 8, wherein the optical components are spatially grouped on the image mapping field unit by mirror facet tilts.
- 25 10. The image mapping spectrometer of claim 6, wherein at least one optical component comprises a prism wedge angle.

11. The image mapping spectrometer of claim 1, wherein the image mapping field unit comprises an array of optical components, and wherein each optical component exhibits an optical power selected from a group consisting of: symmetric, asymmetric, and anamorphic.

12. The image mapping spectrometer of claim 1, wherein the image mapping field unit comprises an array of optical components, and wherein at least one optical component is dynamic.

13. The image mapping spectrometer of claim 2, wherein:
the image mapping field unit comprises an array of optical components;
one or more of the optical components exhibit similar optical properties, thereby
forming a logical group; and
images from each of the optical components in the logical group impinge upon one image sensor.

14. The image mapping spectrometer of claim 1, wherein the spectral separation unit comprises an optical component selected from a group consisting of: a refractive component, and a diffractive component.

15. The image mapping spectrometer of claim 1, wherein the spectral separation unit comprises at least one optical component that is dynamic.

16. The image mapping spectrometer of claim 1, wherein the selective imager comprises:
one or more collecting objectives; and
one or more re-imaging lenses.

17. The image mapping spectrometer of claim 16, wherein at least one collecting objective is capable of receiving a sub-image from the image mapping field unit.

18. The image mapping spectrometer of claim 17, wherein the sub-image comprises less than a complete image.

19. The image mapping spectrometer of claim 16, wherein at least one re-imaging lens is capable of receiving a sub-image from the image mapping field unit, and wherein the sub-image comprises less than a complete image.

20. The image mapping spectrometer of claim 16, wherein each re-imaging lens is capable of creating a sub-image of an optical sample on an image sensors.

21. The image mapping spectrometer of claim 1, wherein the selective imager comprises at least one optical component that is dynamic.

5 22. The image mapping spectrometer of claim 1, wherein the image mapping spectrometer is capable of simultaneous and independent optical and digital zoom.

23. The image mapping spectrometer of claim 1, wherein the image mapping spectrometer is capable of imaging an optical sample in two spatial and one spectral dimensions, and wherein the image mapping spectrometer is capable of simultaneous and independent zoom
10 in all three dimensions.

24. The image mapping spectrometer of claim 1, wherein the image mapping spectrometer is capable of simultaneous and independent zoom in a plurality of regions of interest within an optical sample.

25. The image mapping spectrometer of claim 1, wherein the image mapping
15 spectrometer is capable of parallel data collection of at least about 1 million voxels.

26. The image mapping spectrometer of claim 1, wherein the image mapping spectrometer is capable of changing configuration during operation.

27. The image mapping spectrometer of claim 1, wherein the image mapping field unit does not exhibit spectral separation.

20 28. The image mapping spectrometer of claim 1, wherein the image mapping field unit is capable of super resolution in the spectral domain.

29. The image mapping spectrometer of claim 1, wherein:
the image mapping field unit comprises an array of optical components;
the optical components form a plurality of logical groups of optical components
25 which exhibit similar optical properties;
each logical group is capable of forming a sub-image on an image sensor; and
the sub-images impinge upon at least about 60% of the image sensor.

30. The image mapping spectrometer of claim 1, wherein:

the image mapping field unit comprises an array of optical components;
the optical components form a plurality of logical groups of optical components
which exhibit similar optical properties;
each logical group is capable of forming a sub-image on an image sensor; and
5 the sub-images overlap at the image sensor.

31. A method of spectral imaging comprising:

providing an optical sample;

providing an image mapping spectrometer, wherein the image mapping
spectrometer comprises:

10 an image mapping field unit;

a spectral separation unit; and

a selective imager; and

imaging the optical sample with the image mapping spectrometer.

32. The method of spectral imaging of claim 31, wherein the image mapping
15 spectrometer further comprises at least one image sensor

33. The method of claim 32, wherein imaging the optical sample comprise mapping
an image onto one or more of the at least one image sensors.

34. The method of spectral imaging of claim 32, wherein each image sensor
comprises an array of quantitative electromagnetic radiation detectors.

20 35. The method of spectral imaging of claim 32, wherein each image sensor is two-
dimensional.

36. The method of spectral imaging of claim 33, wherein imaging the optical sample
further comprises acquiring a 3D (x, y, λ) datacube; and wherein mapping an image onto the
image sensor comprises displaying the datacube.

25 37. The method of spectral imaging of claim 36, wherein acquiring and displaying the
datacube occurs at a rate of at least about one image per second.

38. The method of spectral imaging of claim 31, wherein:

the image mapping field unit comprises an array of optical components;

the optical components form a plurality of logical groups of optical components which exhibit similar optical properties; and

each logical group forms a sub-image on one or more of the at least one image sensors.

5 39. The method of spectral imaging of claim 31, wherein:
the selective imager comprises:

one or more collecting objectives; and

one or more re-imaging lenses; and

crosstalk in the selective imager is no greater than about 1%.

10 40. The method of spectral imaging of claim 31, further comprising changing a configuration of the image mapping spectrometer without disturbing the optical sample.

41. The method of spectral imaging of claim 31, further comprising optically zooming at least a region of interest of the optical sample.

15 42. The method of spectral imaging of claim 31, further comprising digitally zooming at least a region of interest of the optical sample.

43. The method of spectral imaging of claim 31, wherein the optical sample provides electromagnetic radiation from at least one regime selected from the group consisting of: ultraviolet, visible, near infrared, midwave infrared, long-wave infrared, and any combination thereof.

20 44. The method of spectral imaging of claim 31, wherein the optical sample comprises a tissue sample.

45. The method of spectral imaging of claim 31, wherein the optical sample comprises a fluorescence microscopy image.

25 46. The method of spectral imaging of claim 31, wherein the optical sample comprises a reflectance microscopy image.

47. The method of spectral imaging of claim 31, wherein the optical sample comprises a transmission microscopy image.

48. The method of spectral imaging of claim 31, wherein the image mapping spectrometer further comprises an optical element capable of endoscopic imaging.

49. The method of spectral imaging of claim 48, wherein the optical element comprises at least one optical element selected from the group consisting of: a grin lens, a
5 coherent multi fiber bundle, an incoherent multi fiber bundle, a miniature objective, a miniature lens, and any combination thereof.

50. The method of spectral imaging of claim 31, further comprising transmitting data to a remote location.

51. The method of spectral imaging of claim 31, wherein the optical sample
10 comprises a food component sample.

52. The method of spectral imaging of claim 31, wherein the optical sample comprises a retinal image.

53. A method of fabricating image mapping field units comprising:
(a) providing an image mapping field unit substrate;
15 (b) providing an optical component cross section profile;
(c) providing a surface shaped diamond tool specific to the optical component cross section profile; and
(d) utilizing the surface shaped diamond tool to create the optical component cross section profile in the image mapping field unit substrate to form a mapping element.

20 54. The method of fabricating image mapping field units of claim 53, further comprising:
utilizing the mapping element to create a mold; and
molding additional mapping elements.

55. The method of fabricating image mapping field units of claim 53, wherein the
25 substrate comprises a compound selected from a group consisting of: an aluminum alloy, a brass compound, a copper compound, a gold compound, a nickel compound, a silver compound, an acrylic compound, a flueoroplastic compound, a polycarbonate compound, and any combination thereof.

56. The method of fabricating image mapping field units of claim 53, further comprising repeating steps (b)-(d) for a plurality of optical component cross section profiles.

57. The method of fabricating image mapping field units of claim 56, wherein the optical component cross section profiles are spatially grouped on the mapping element by mirror
5 facet tilts.

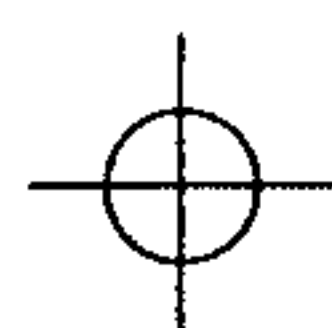


Fig. 1

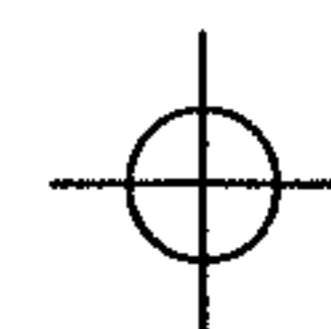
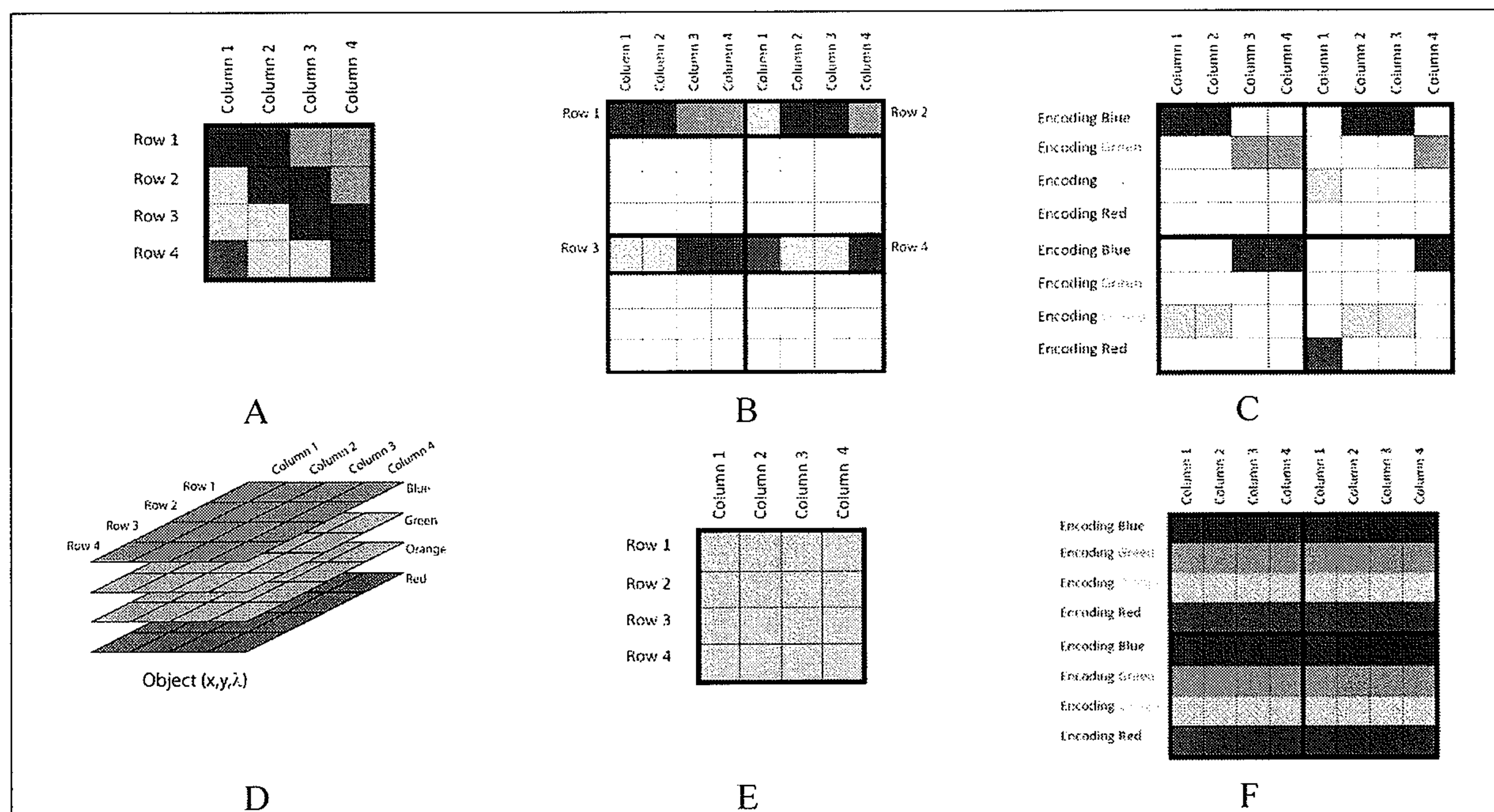
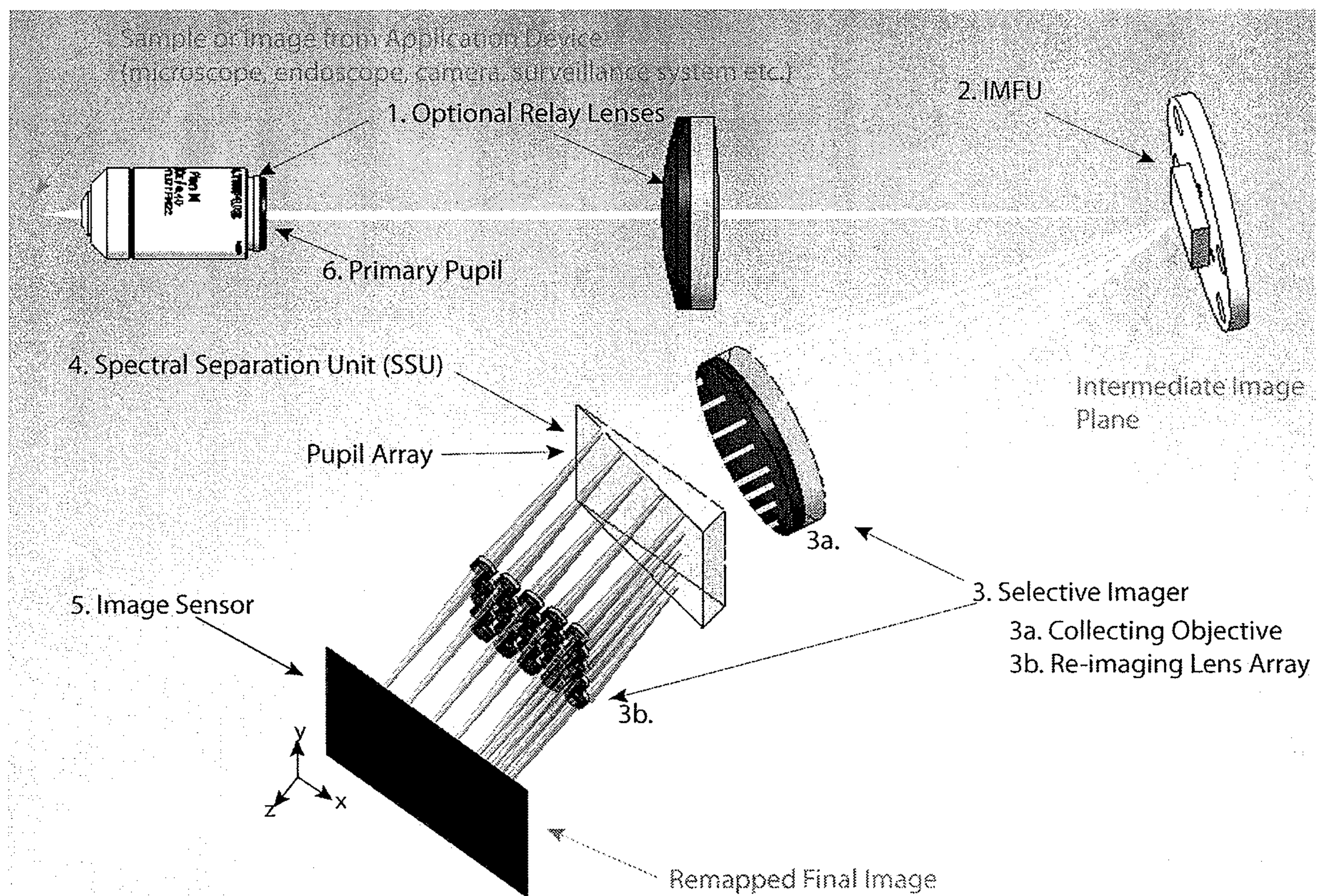


Fig. 2



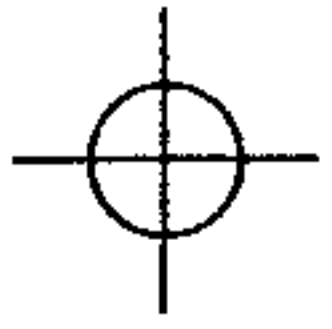
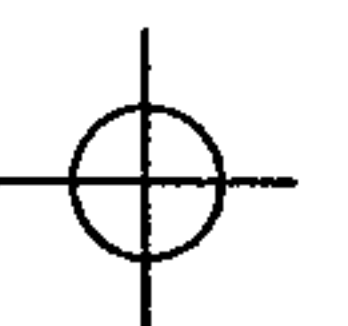
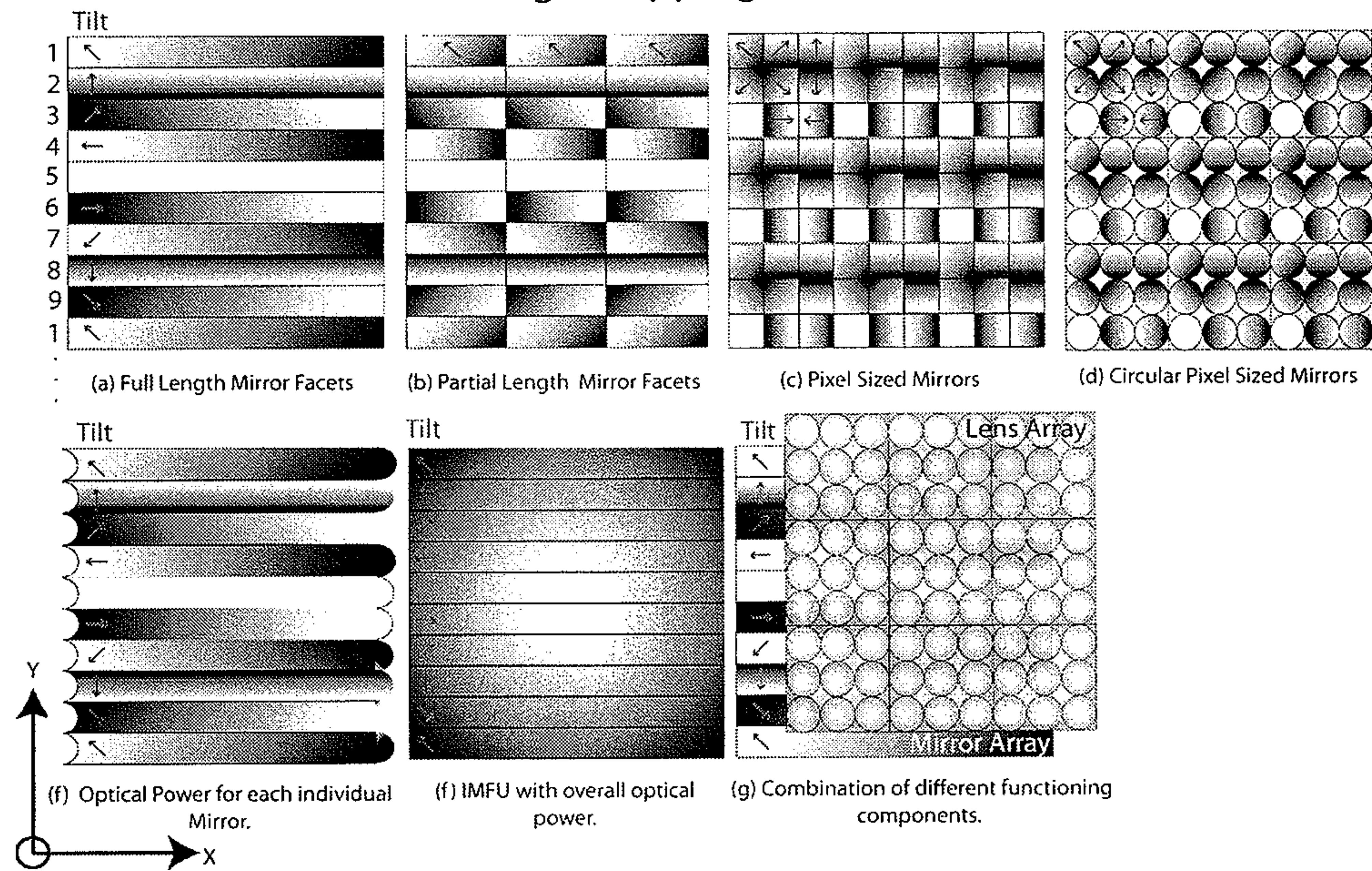


Fig. 3

Image Mapping Field Units



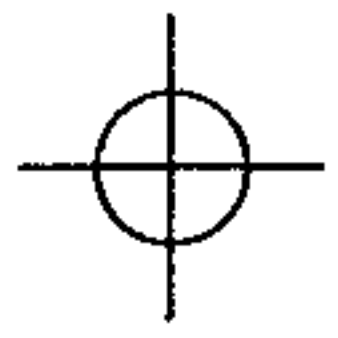
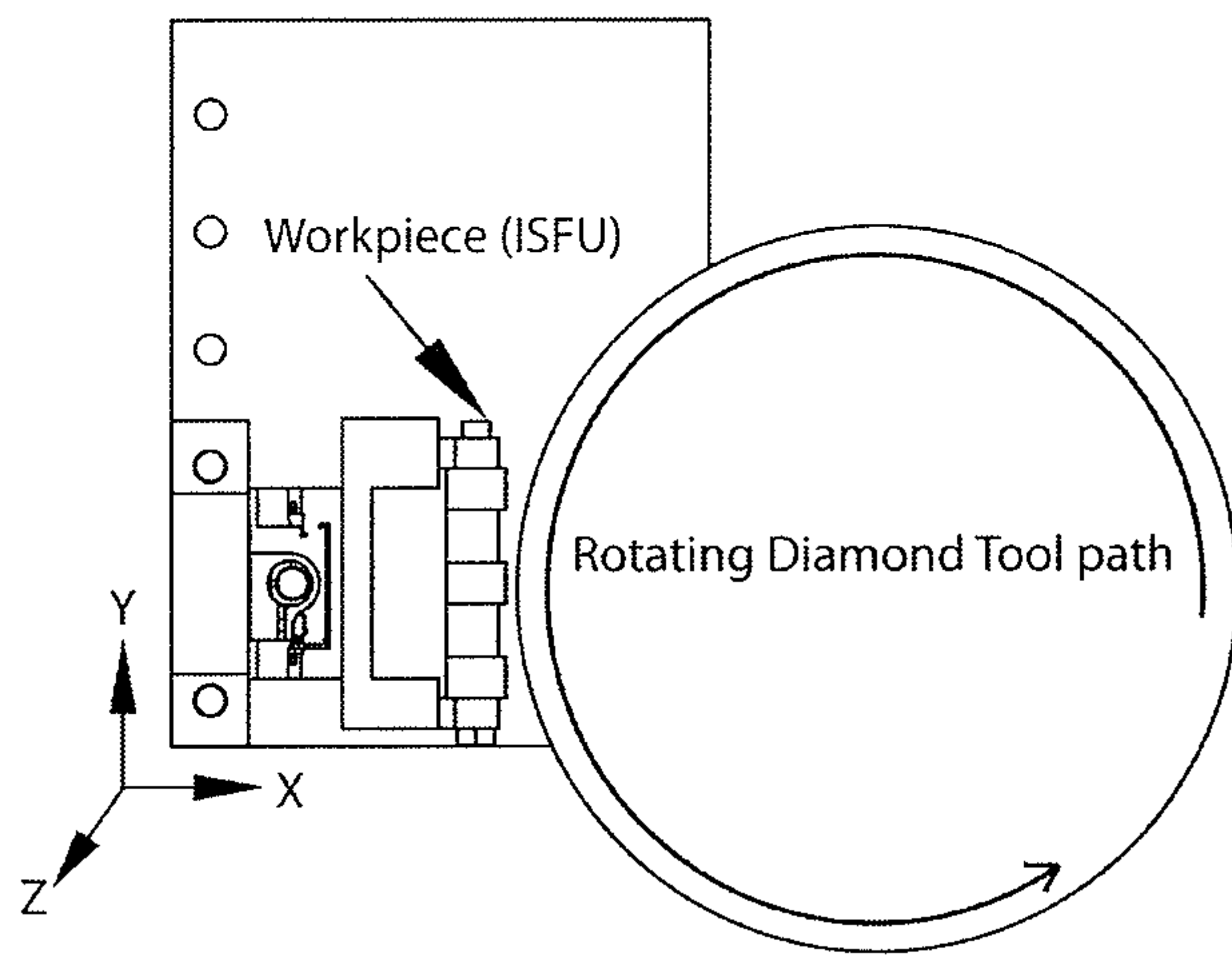
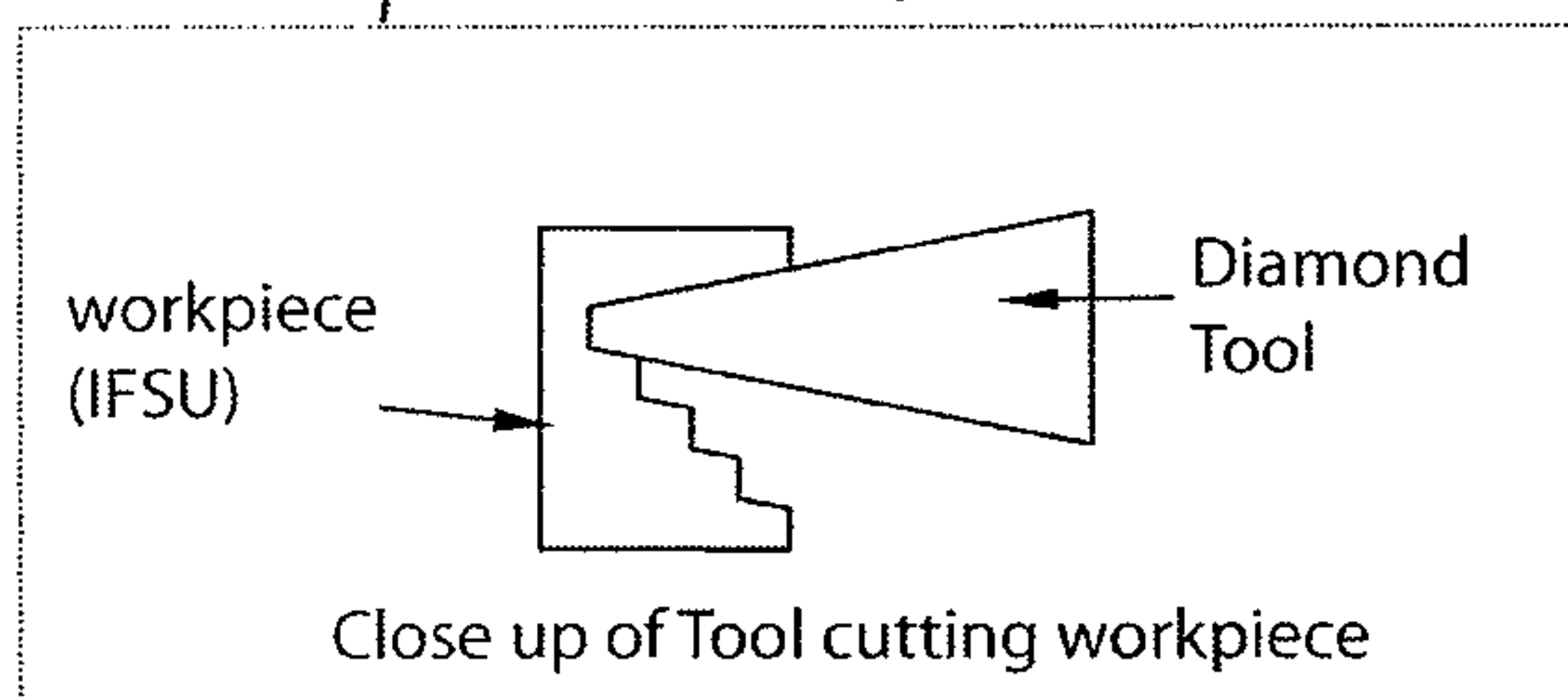
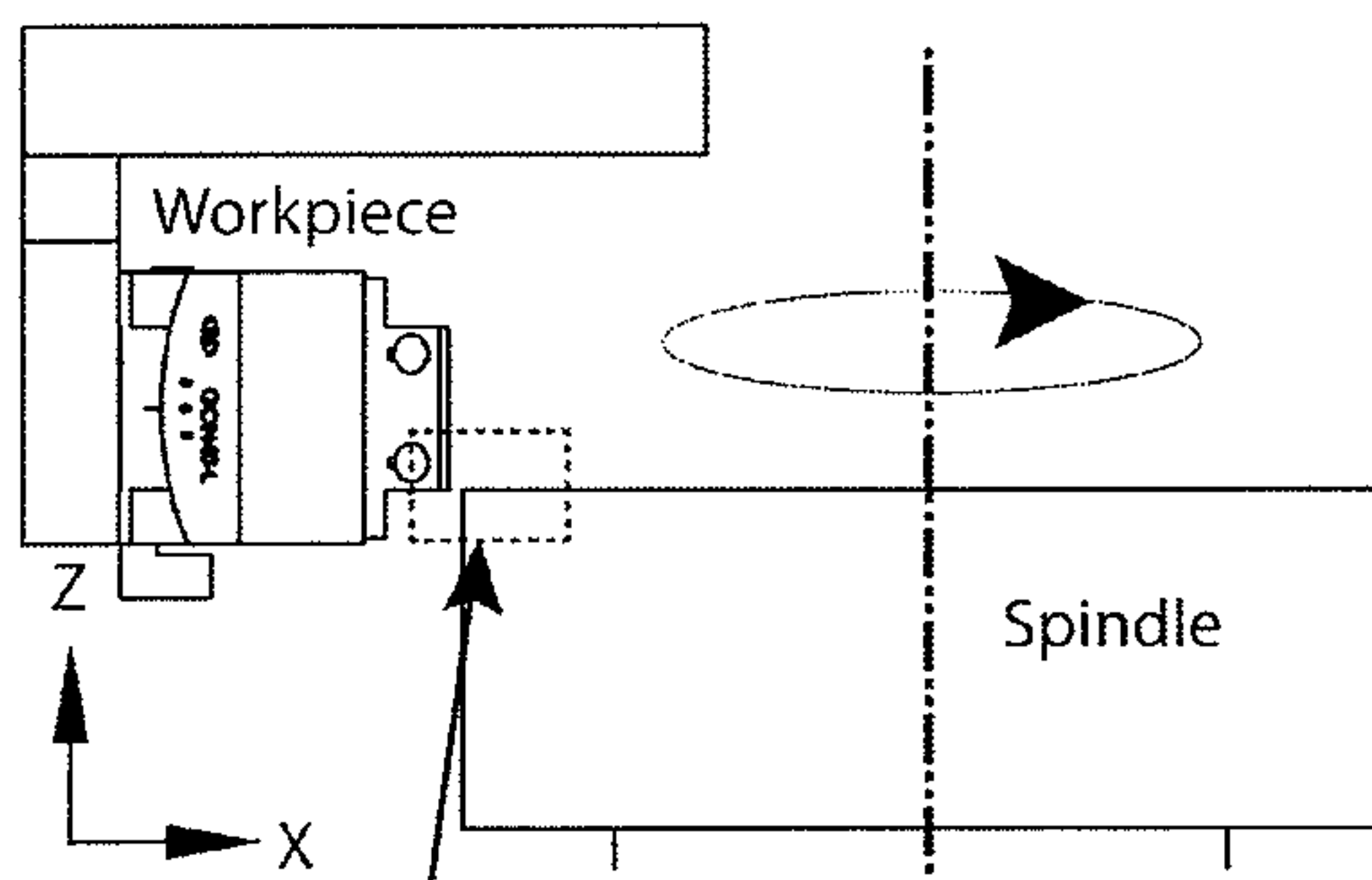


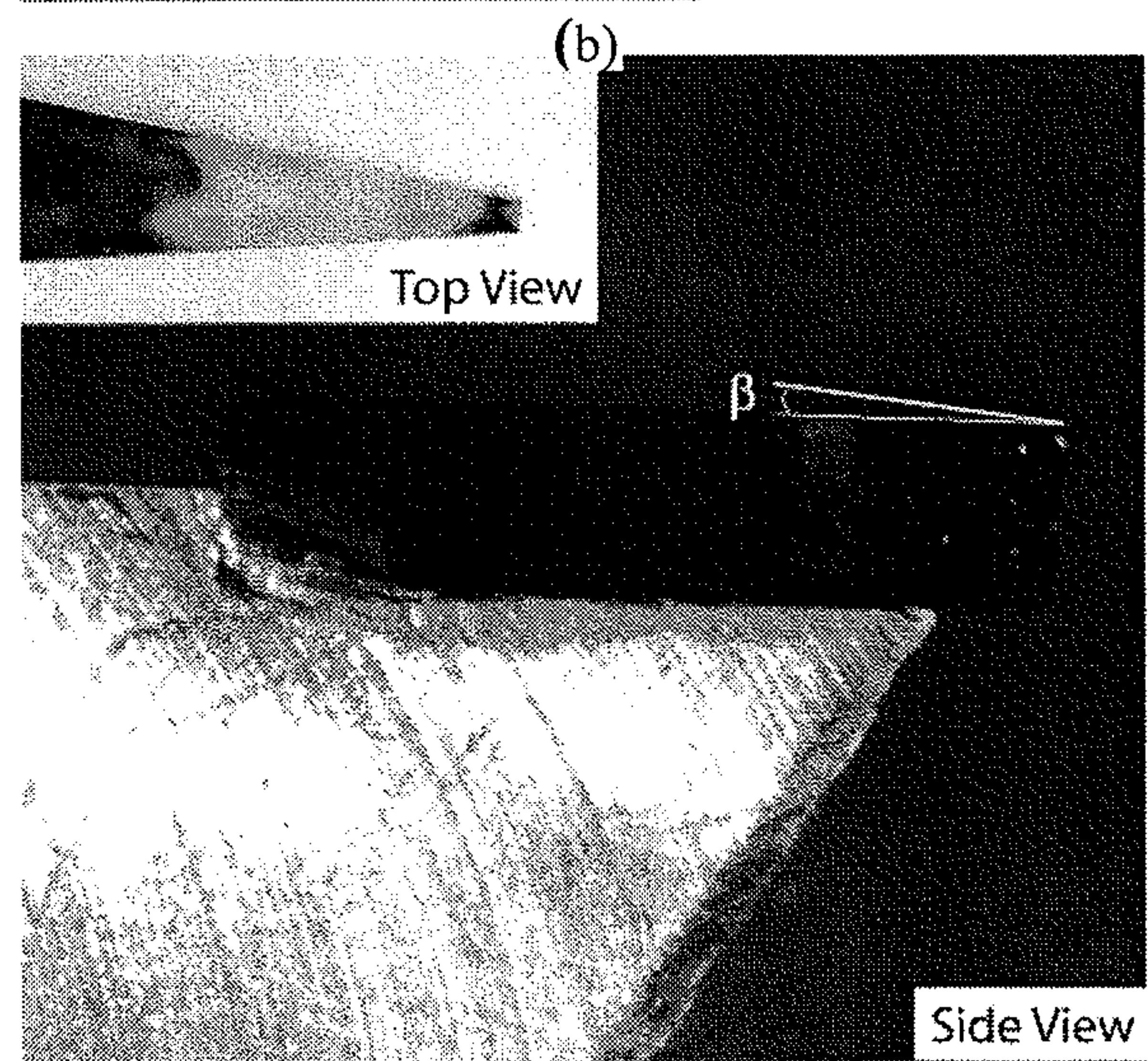
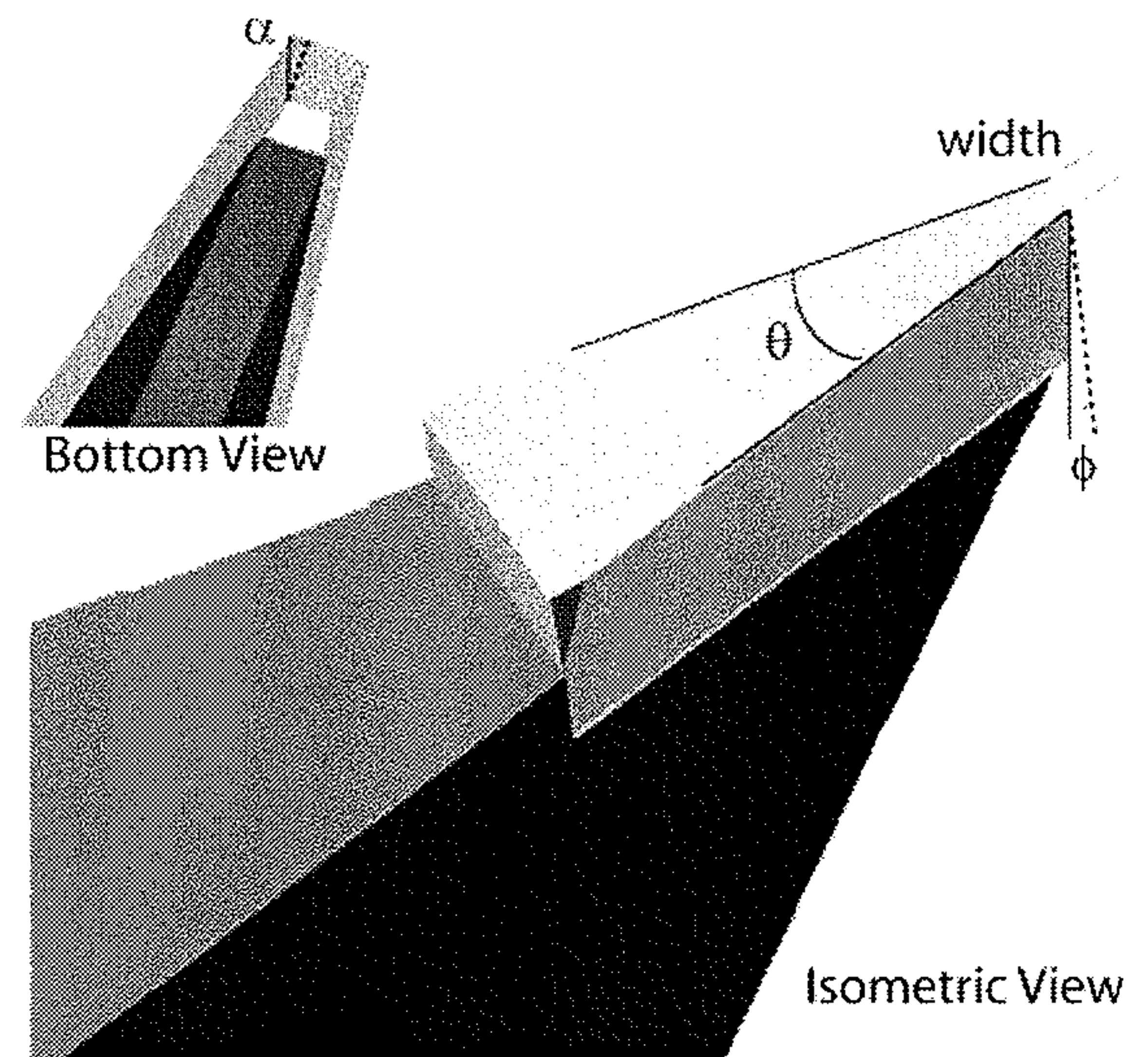
Fig. 4



(a)



(c)



(d)

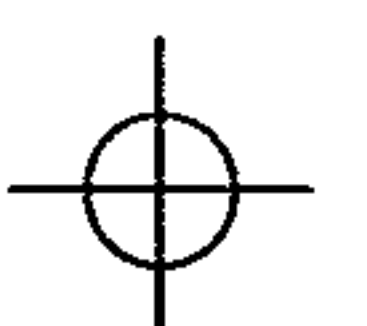
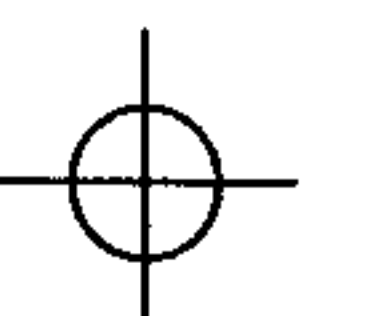
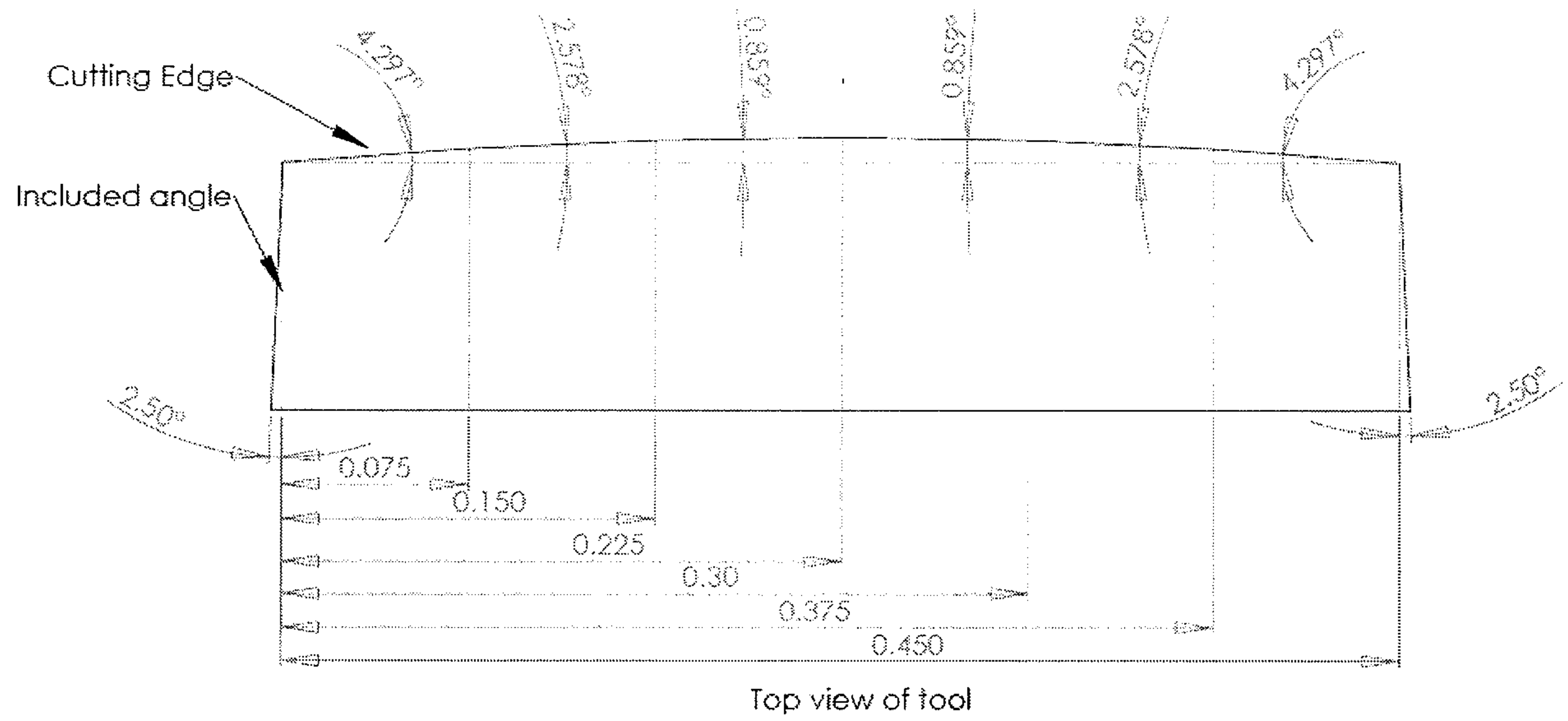




Fig. 5



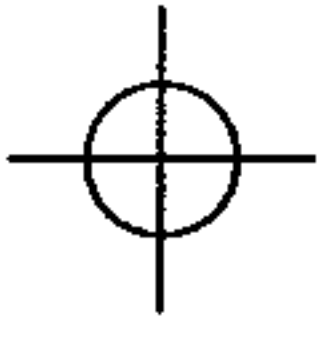
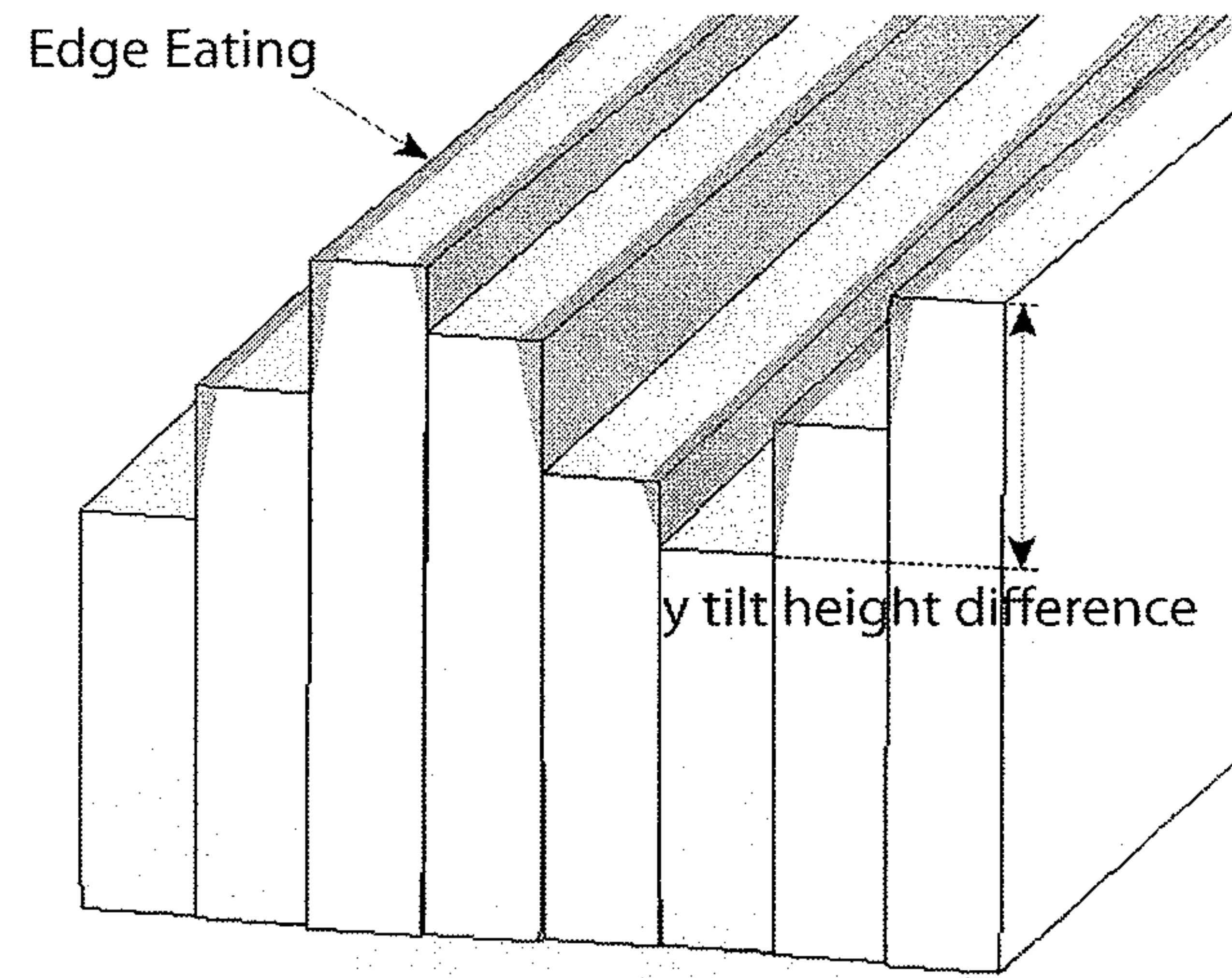
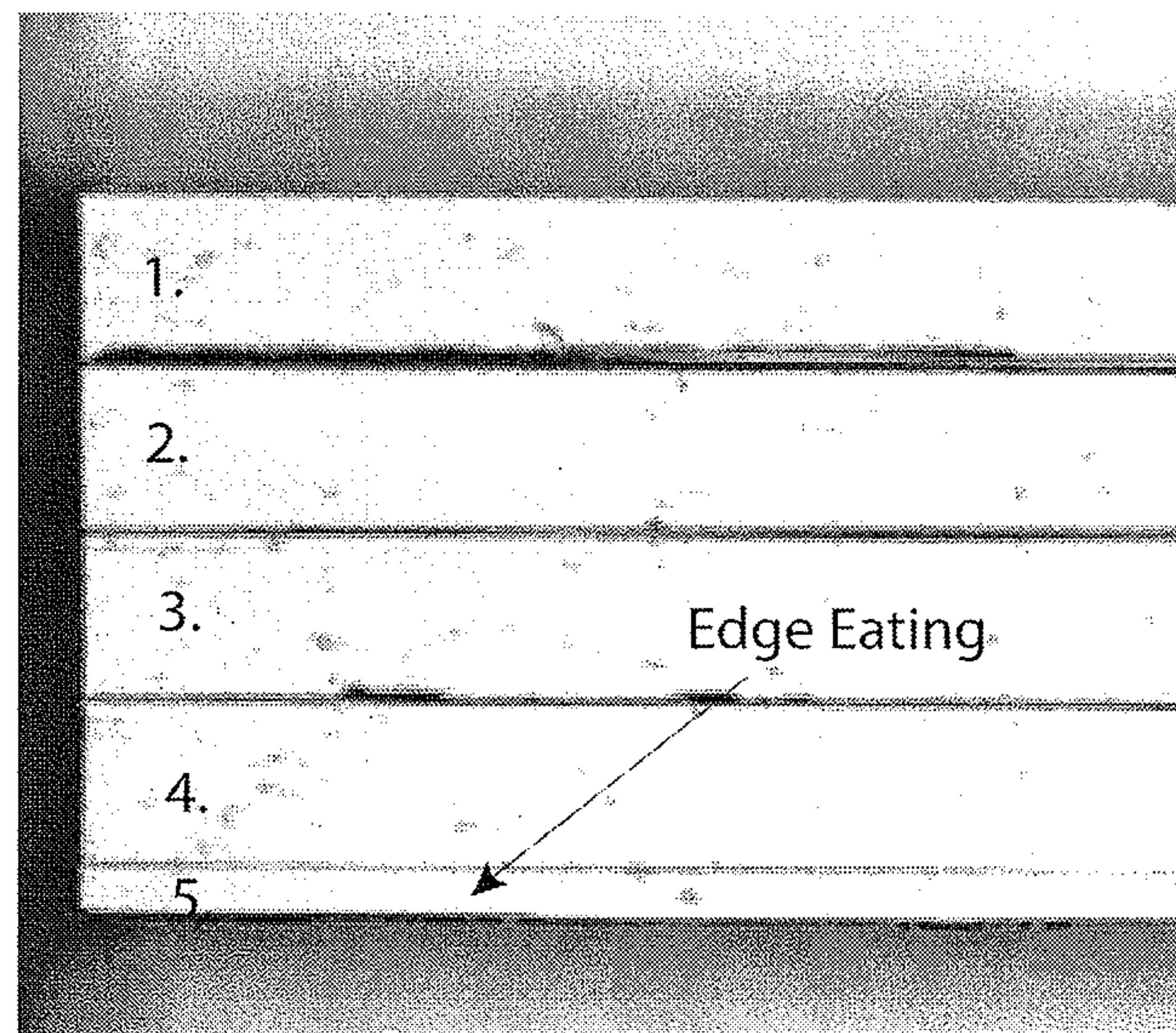


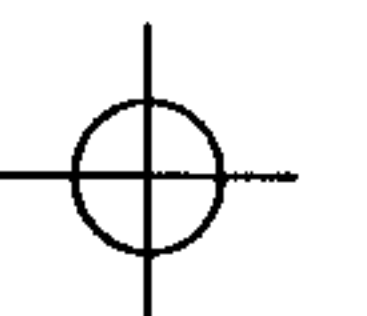
Fig. 6



(a)



(b)



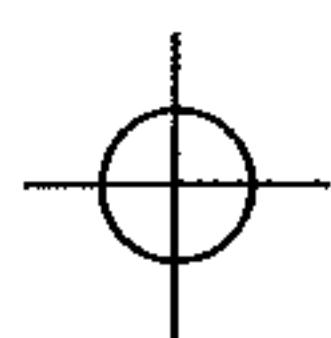
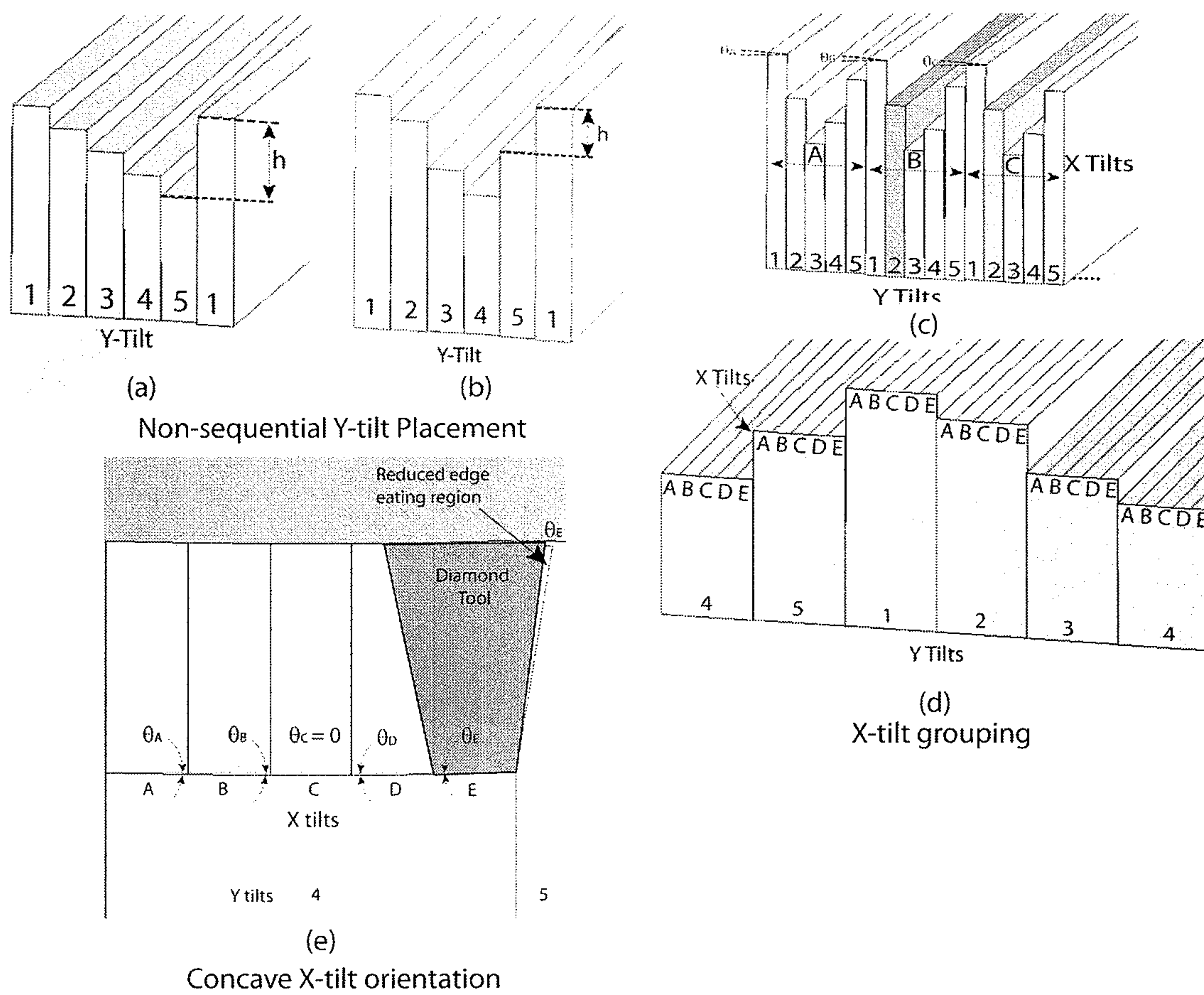


Fig. 7



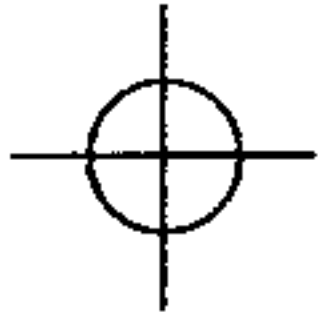
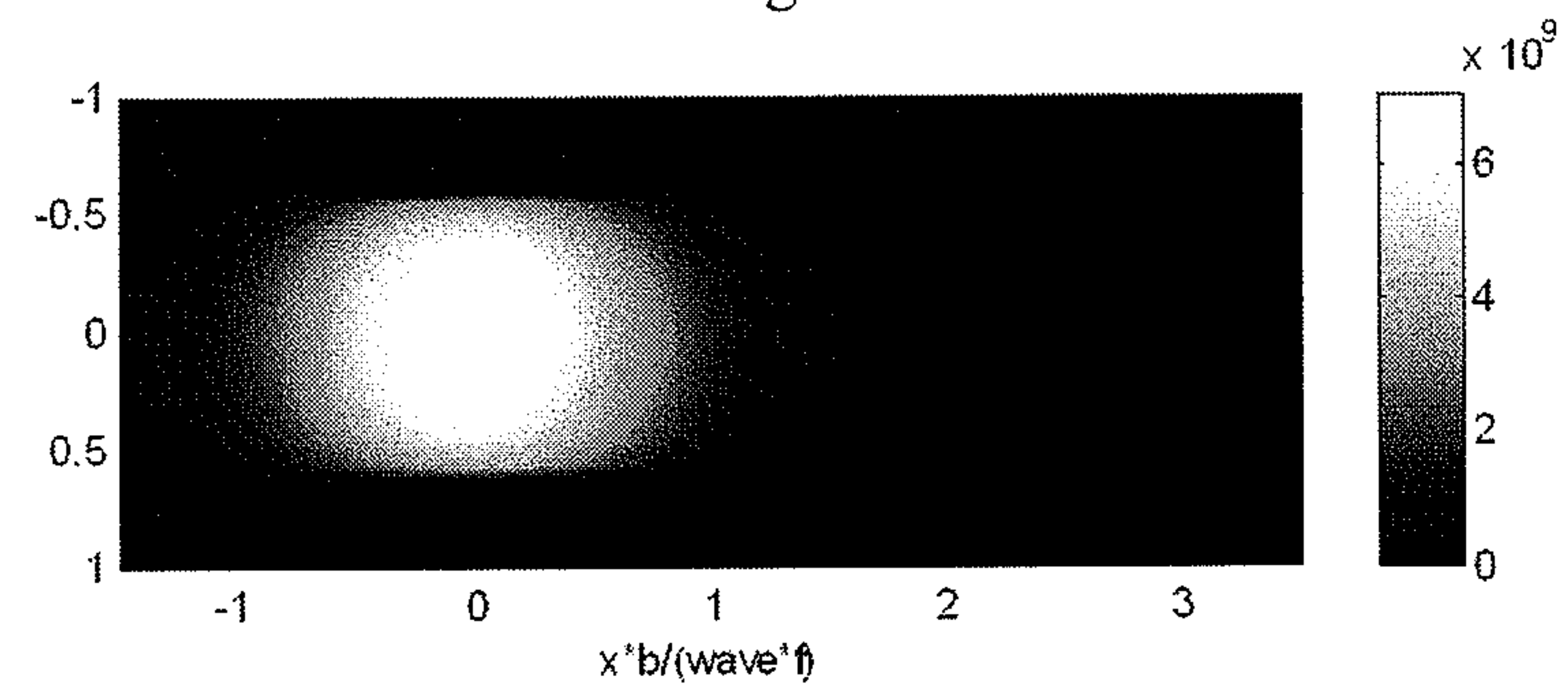
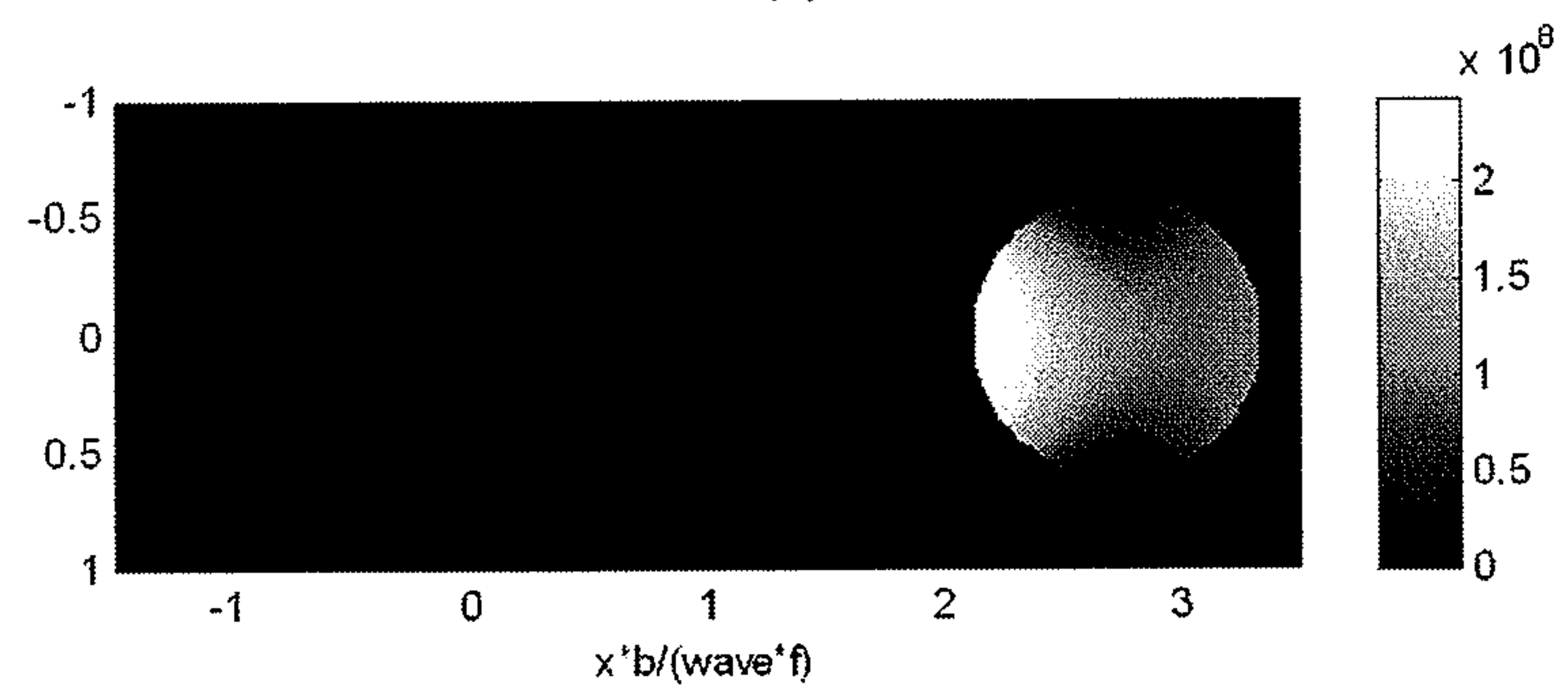


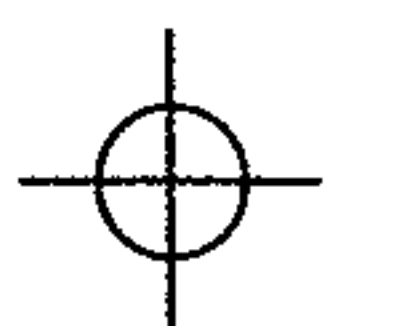
Fig. 8



(a)



(b)



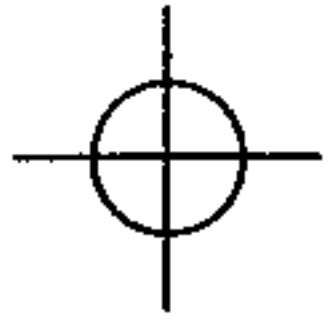


Fig. 9

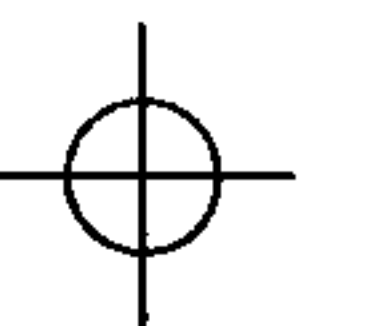
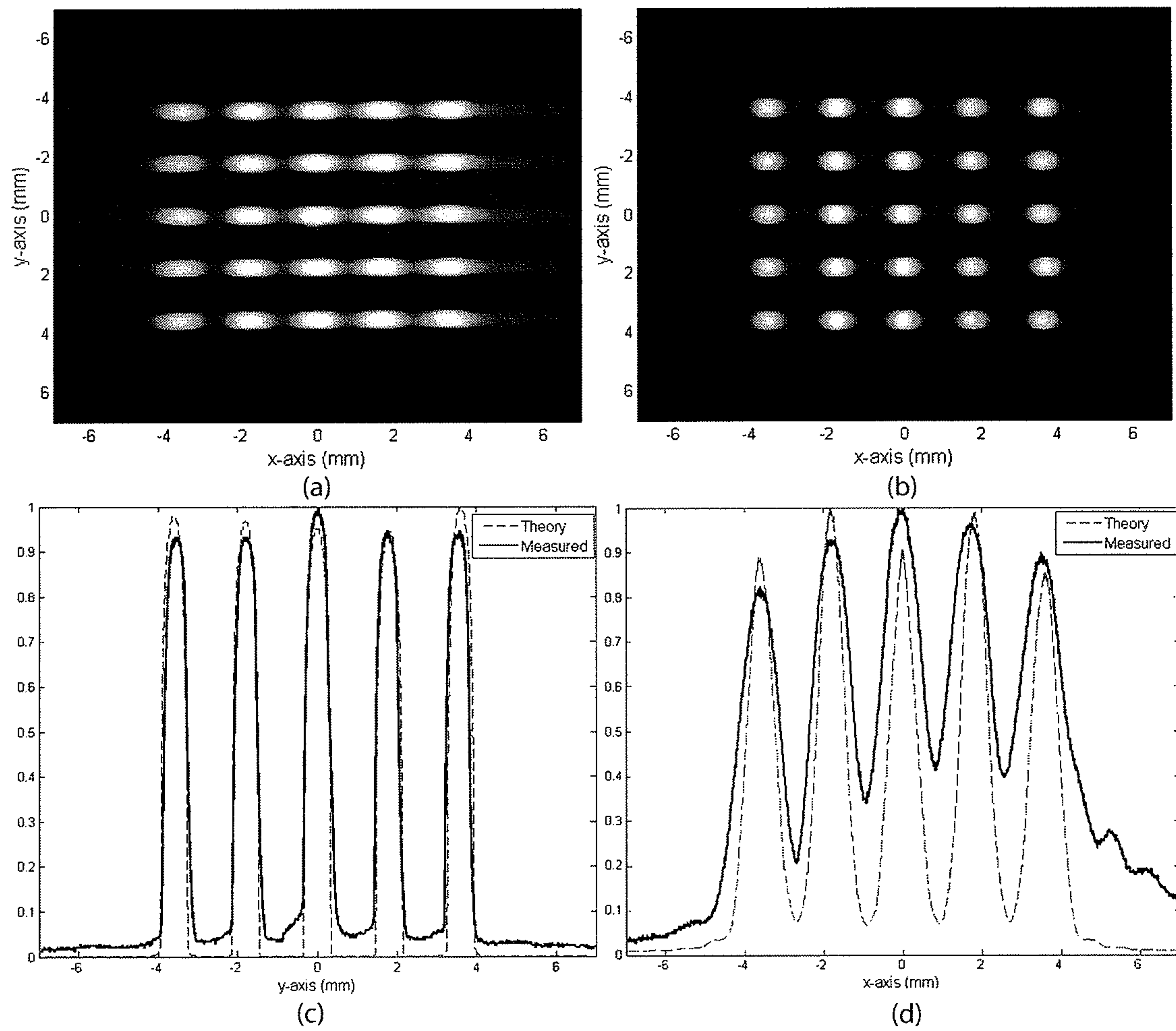
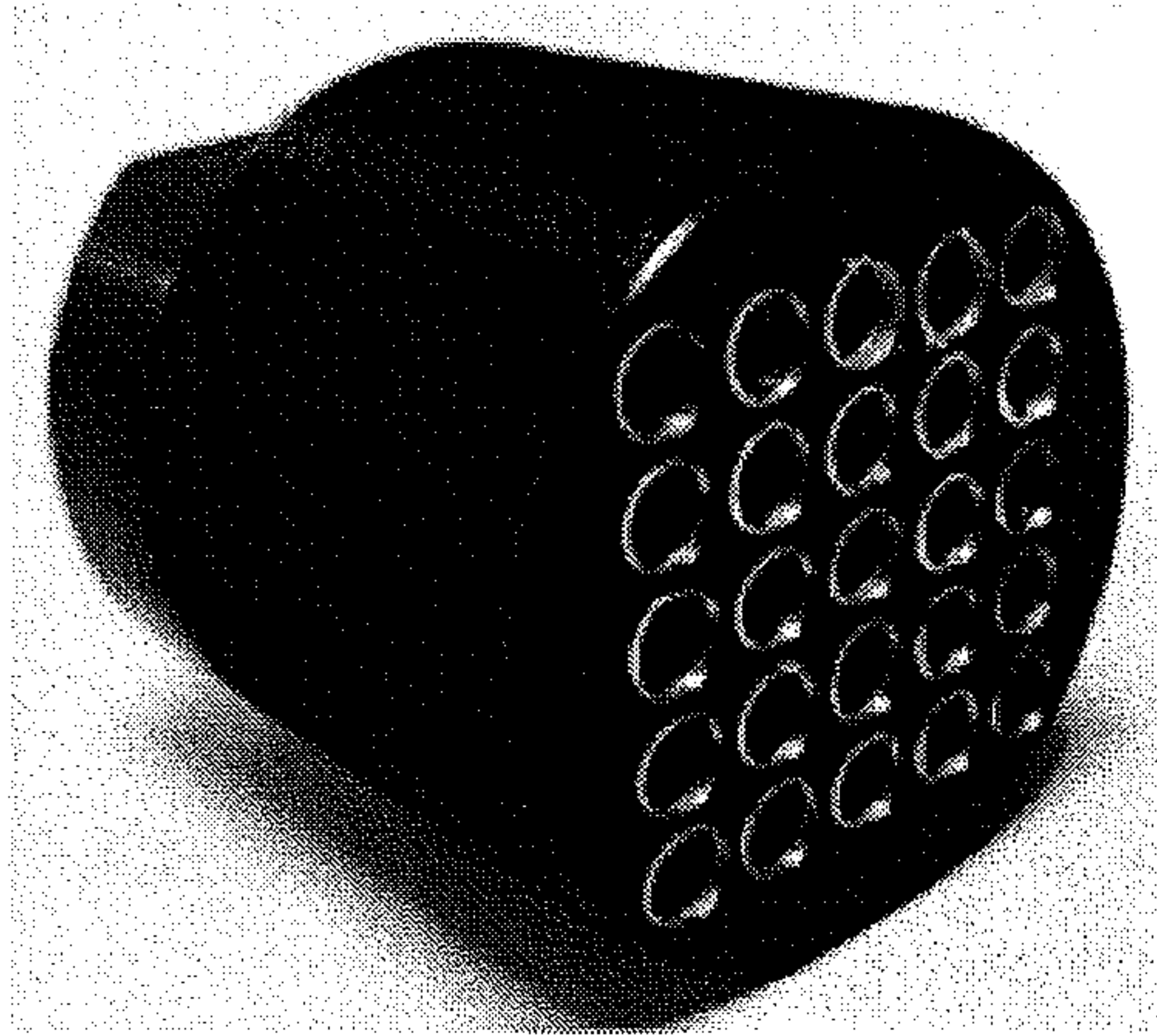
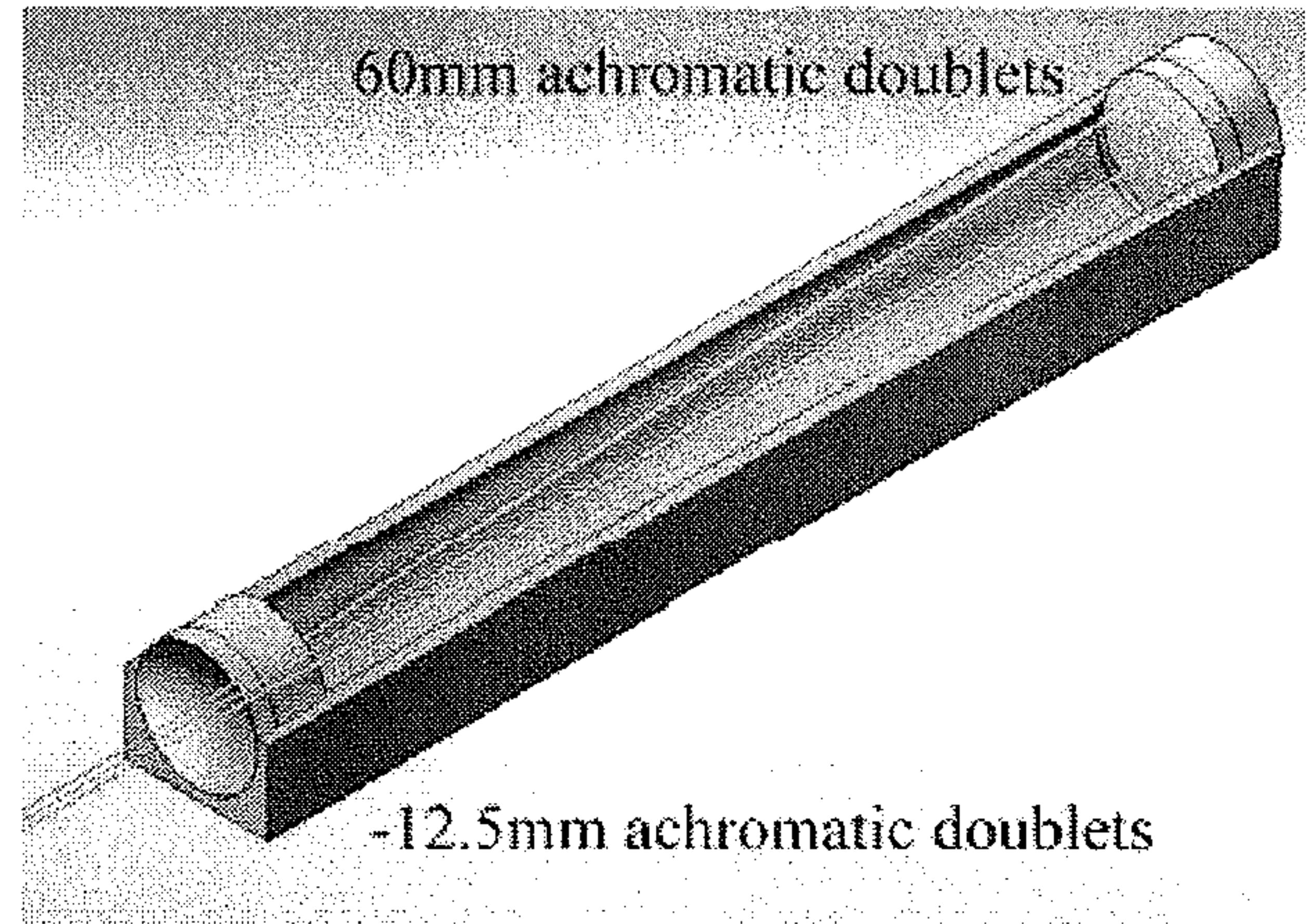




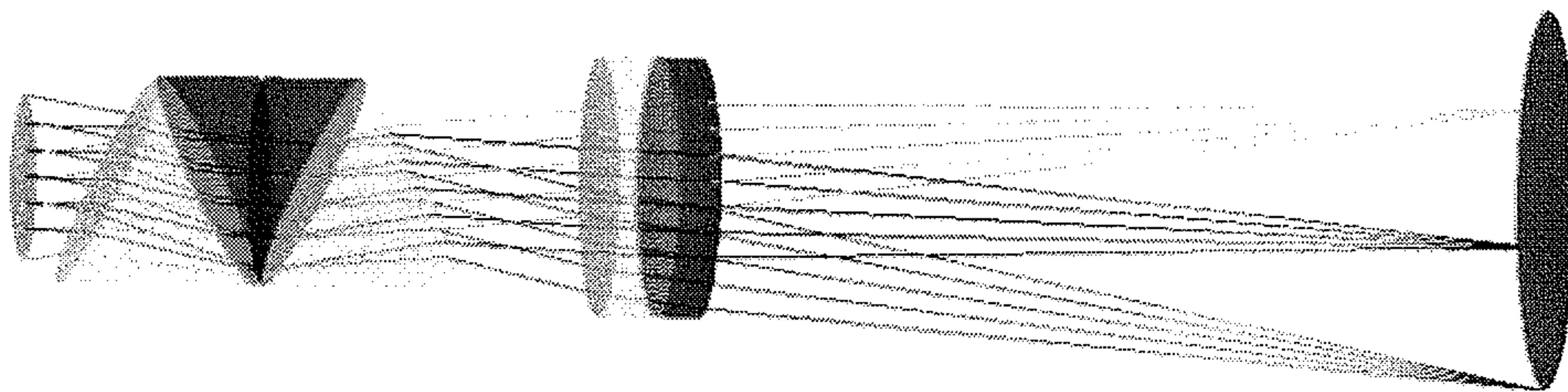
Fig. 10



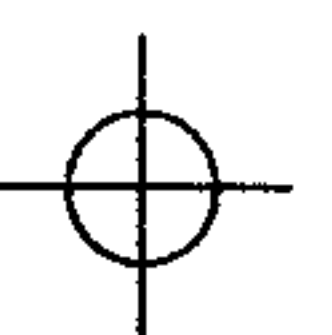
(a)



(b)



(c)



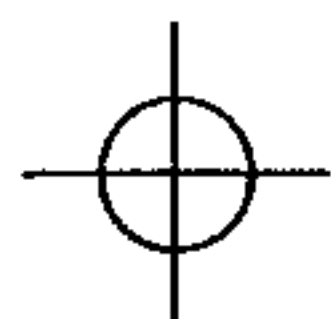
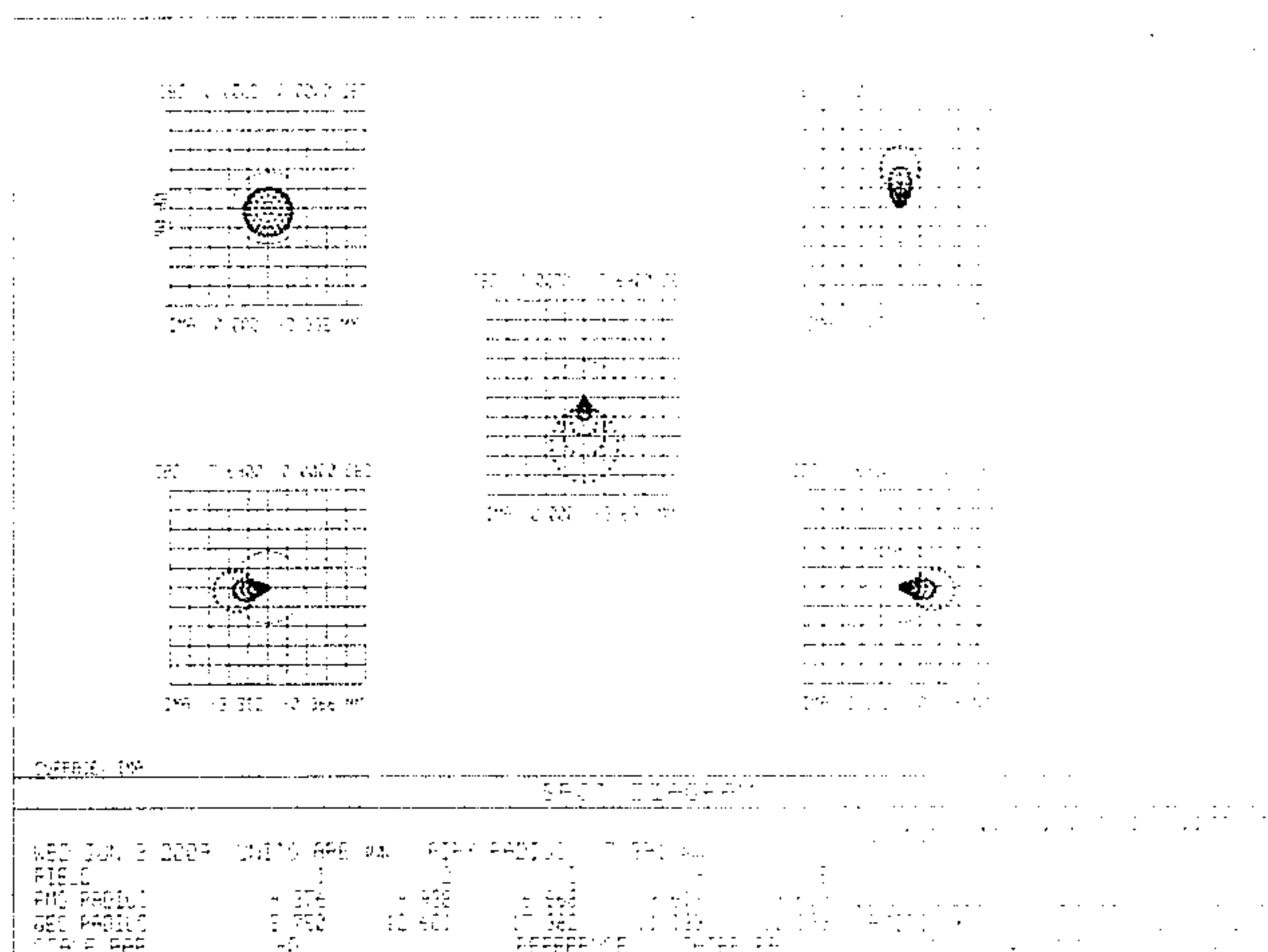
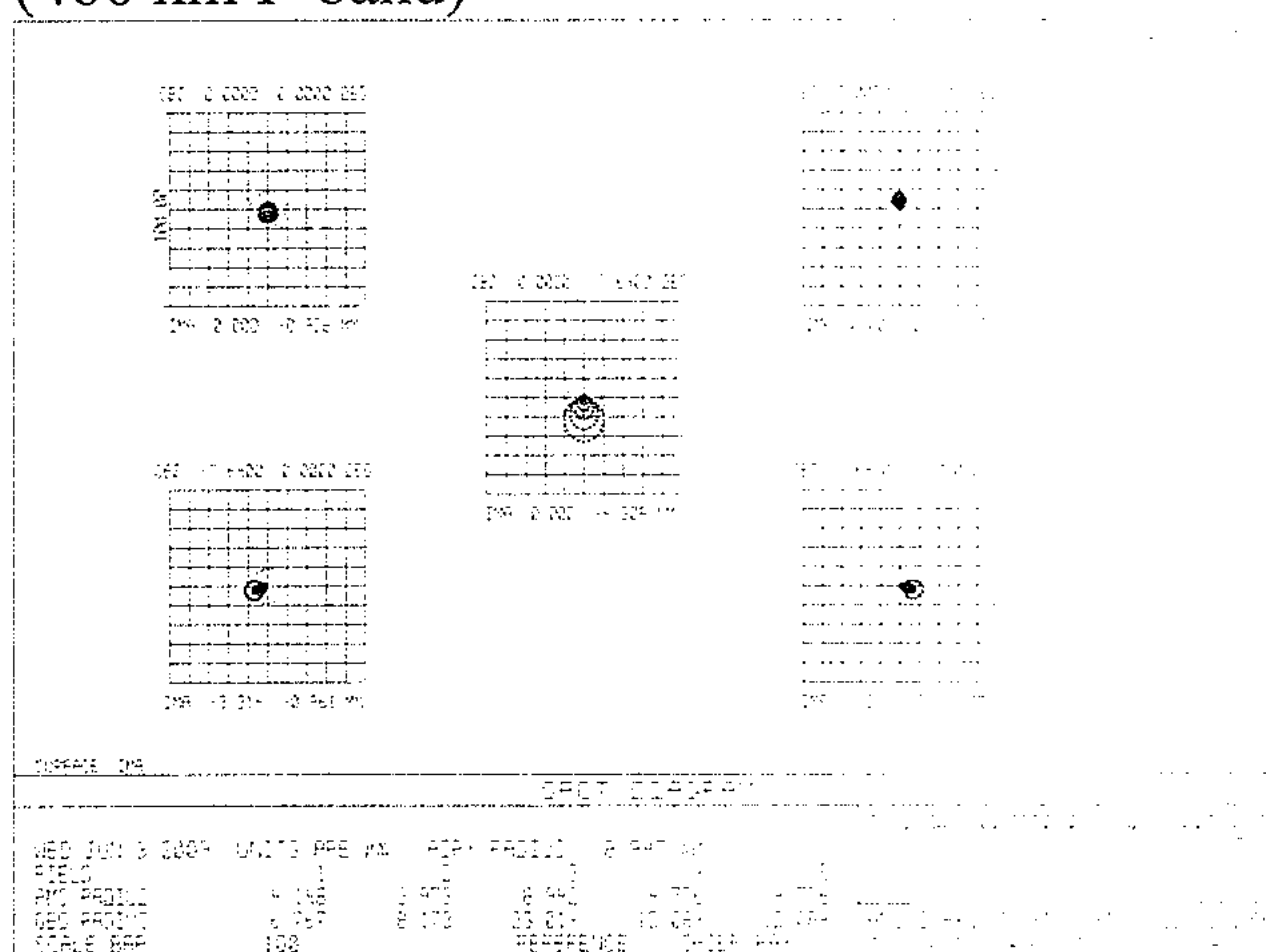


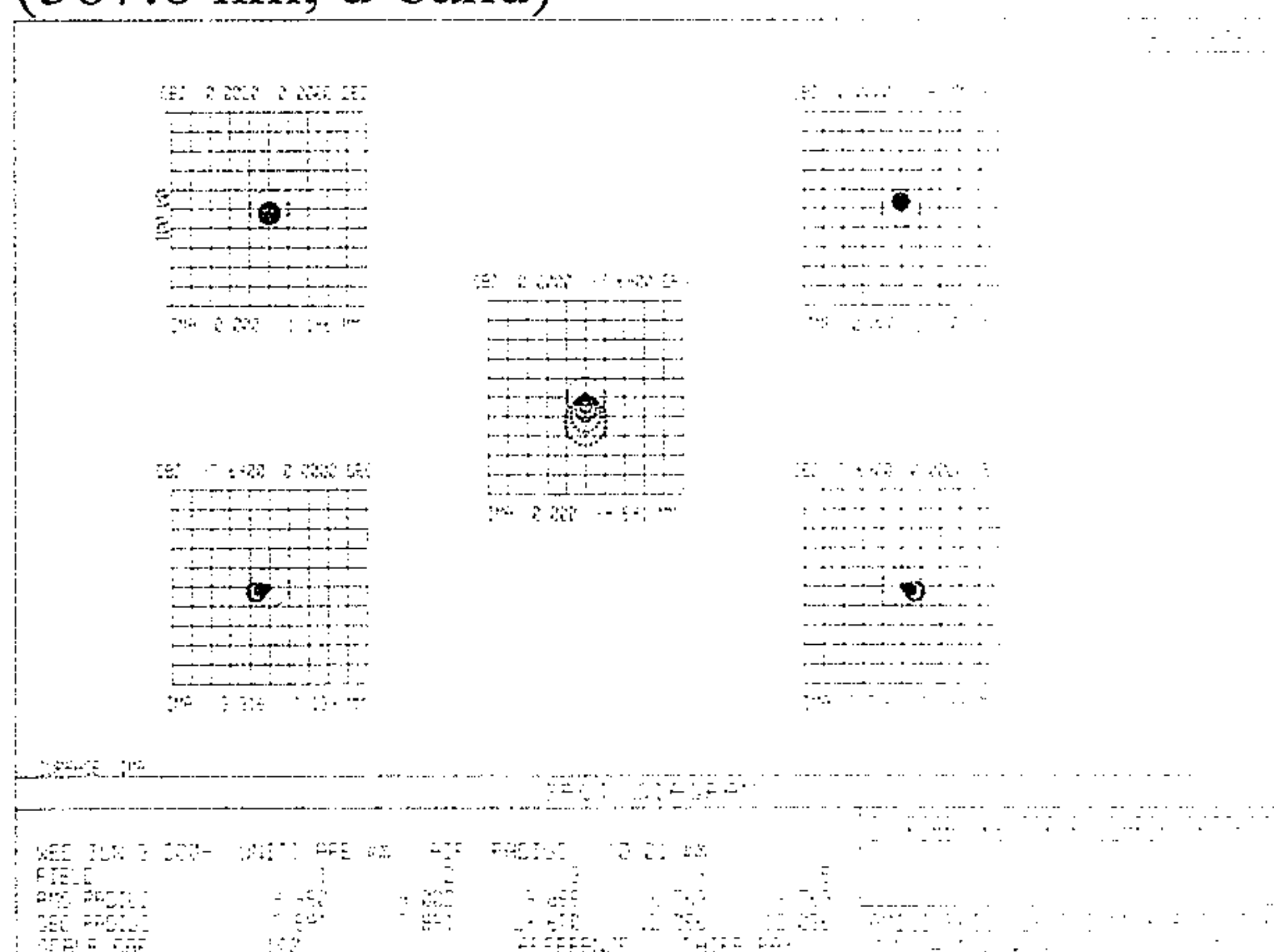
Fig. 11



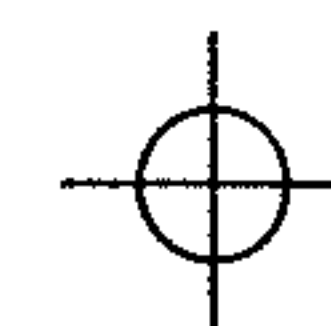
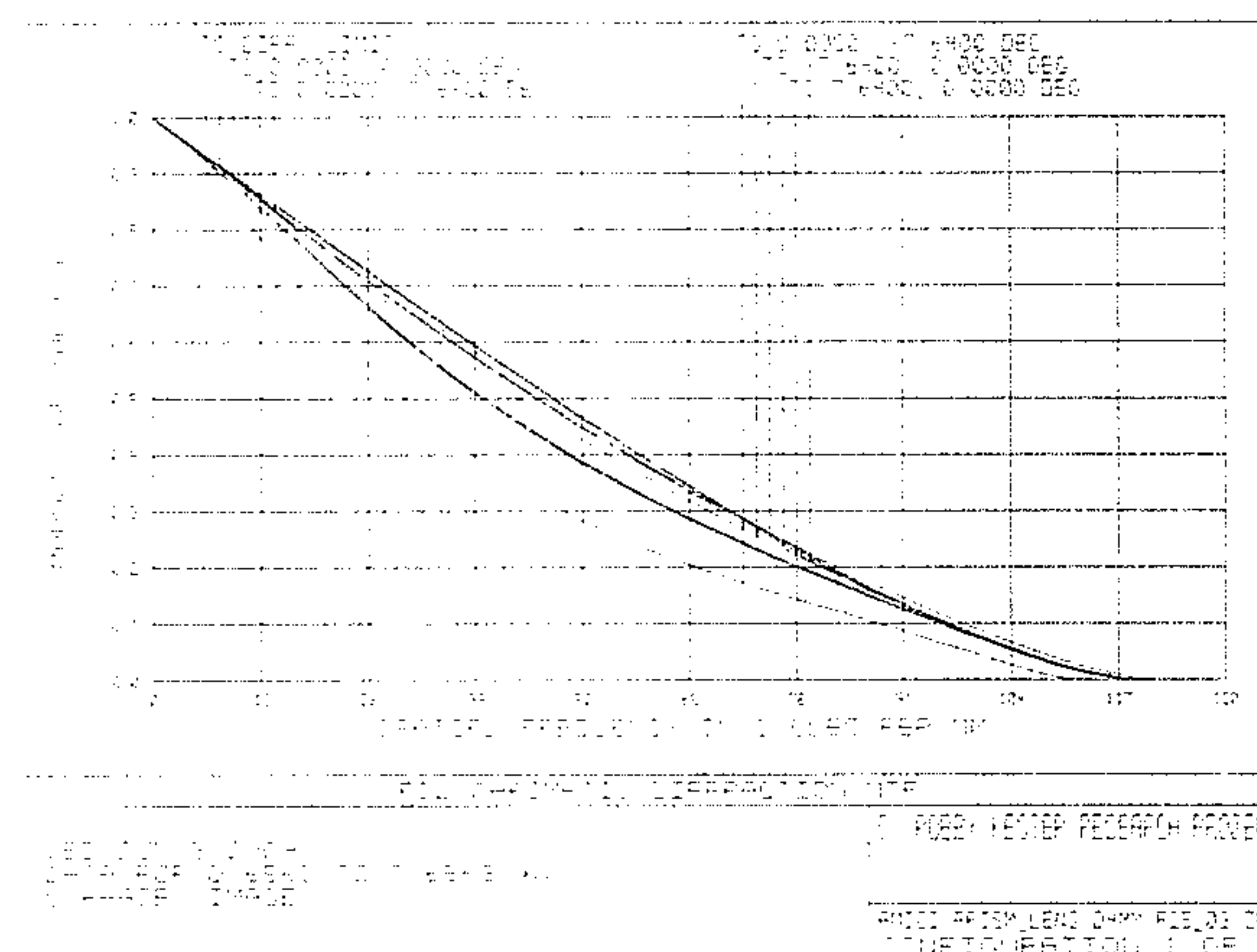
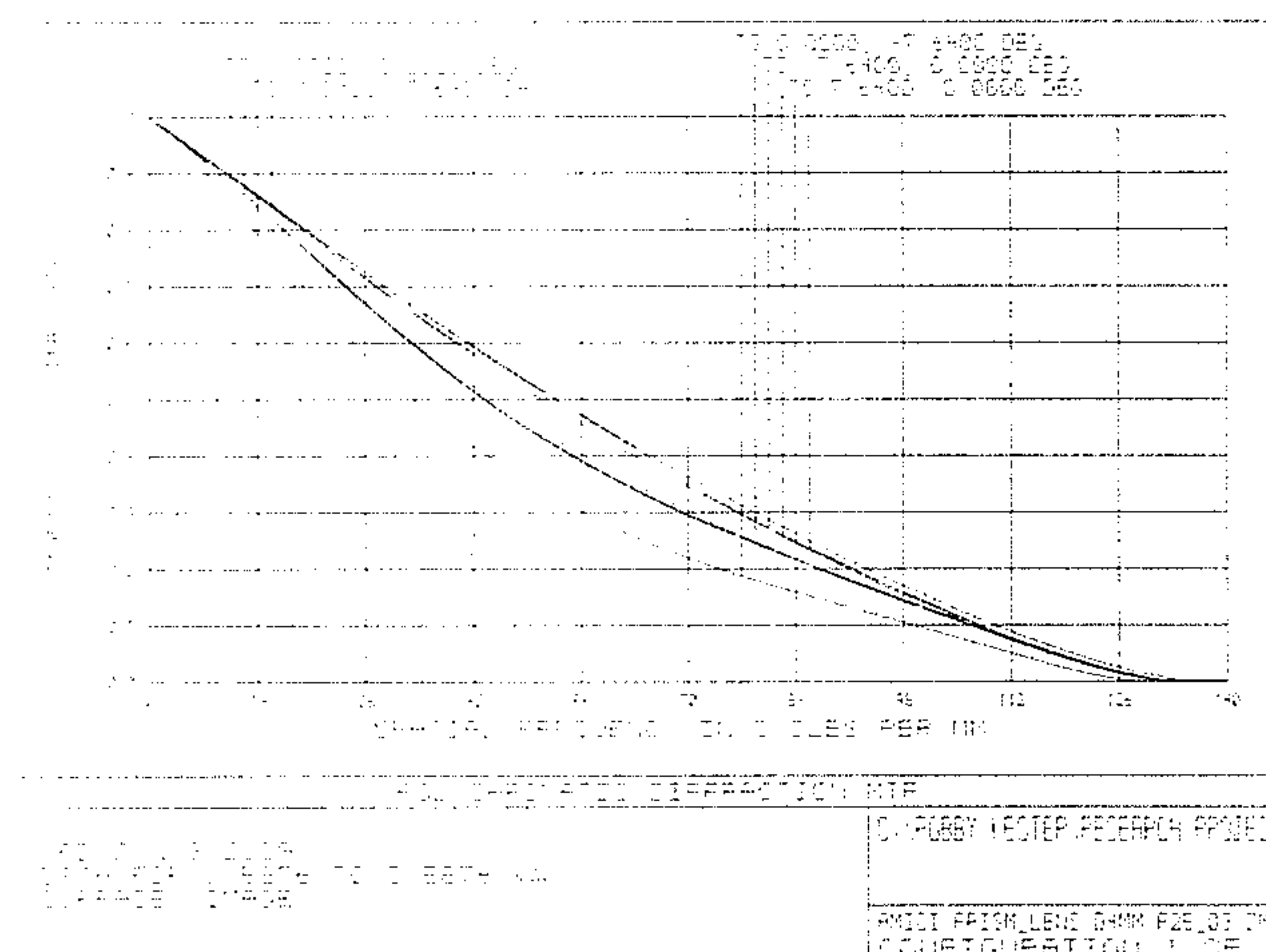
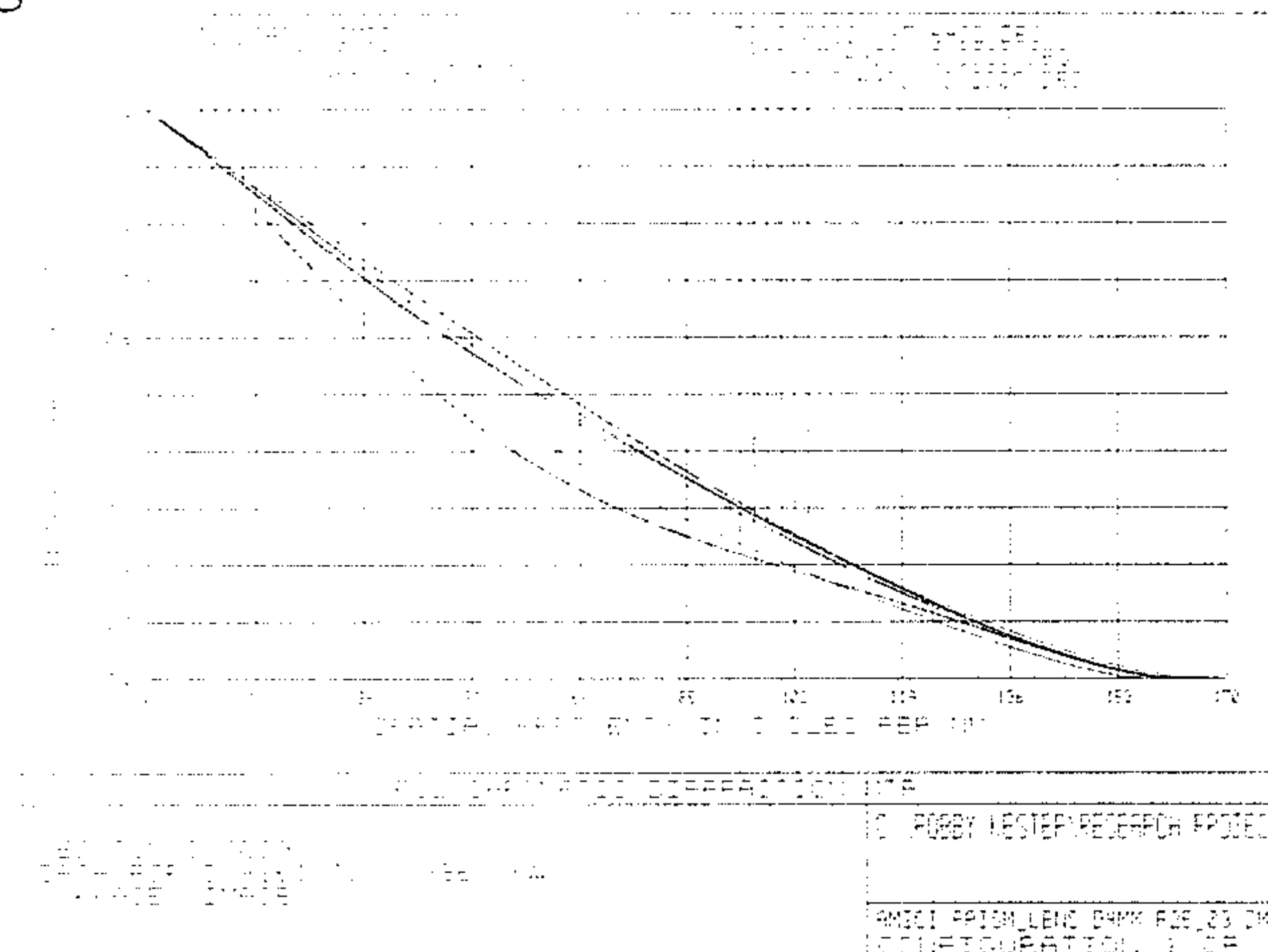
(486 nm F-band)



(587.6 nm, d-band)



(656.3nm, C-band)



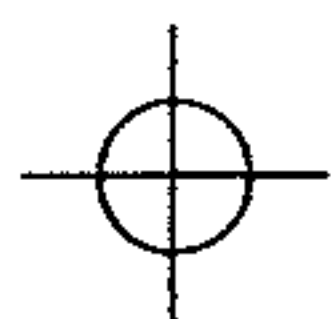
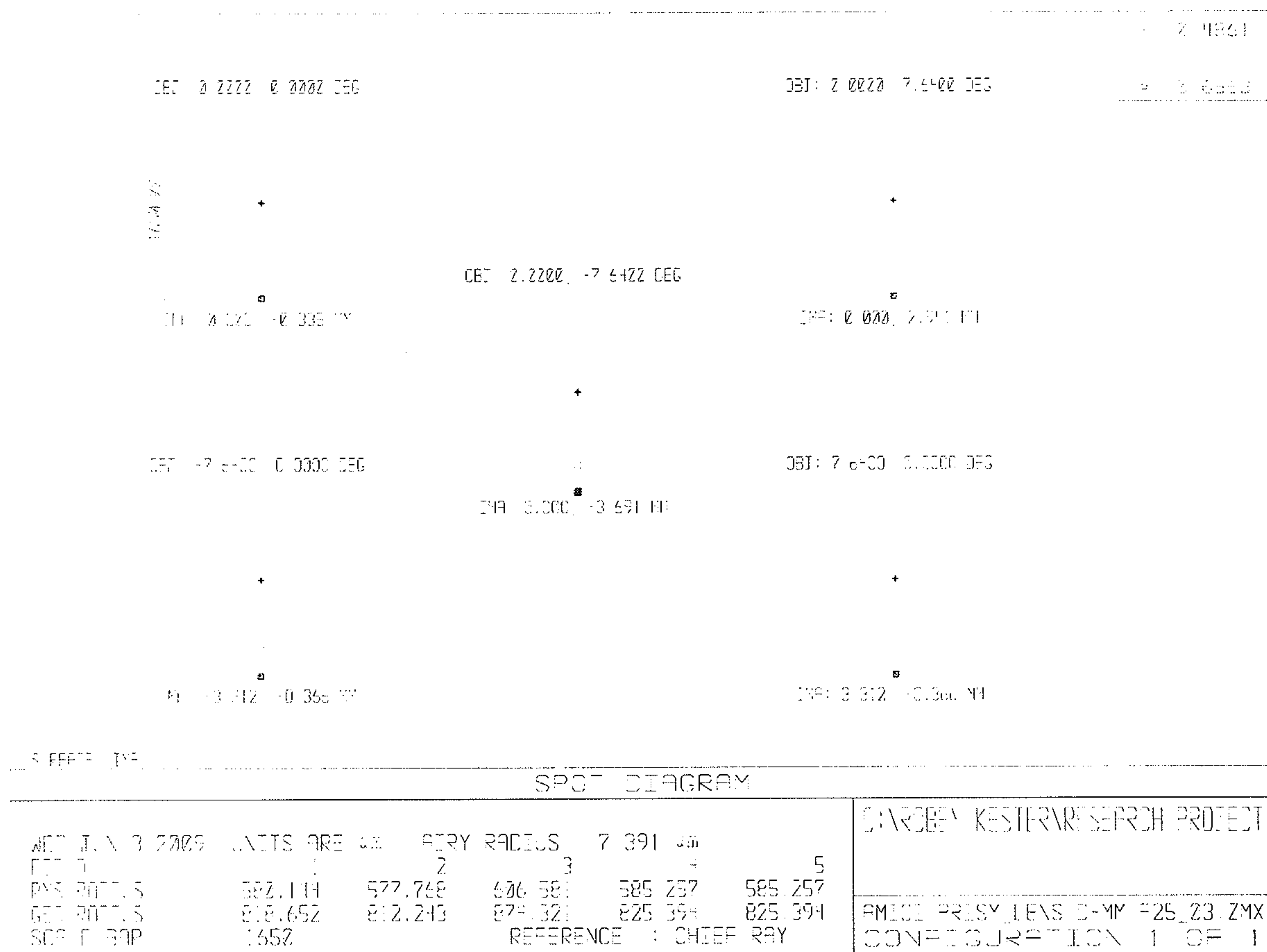


Fig. 12



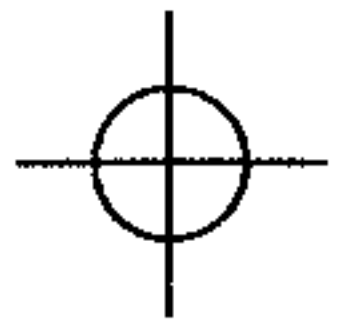
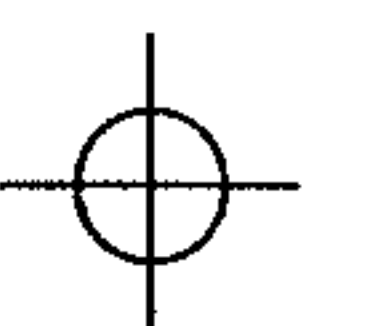
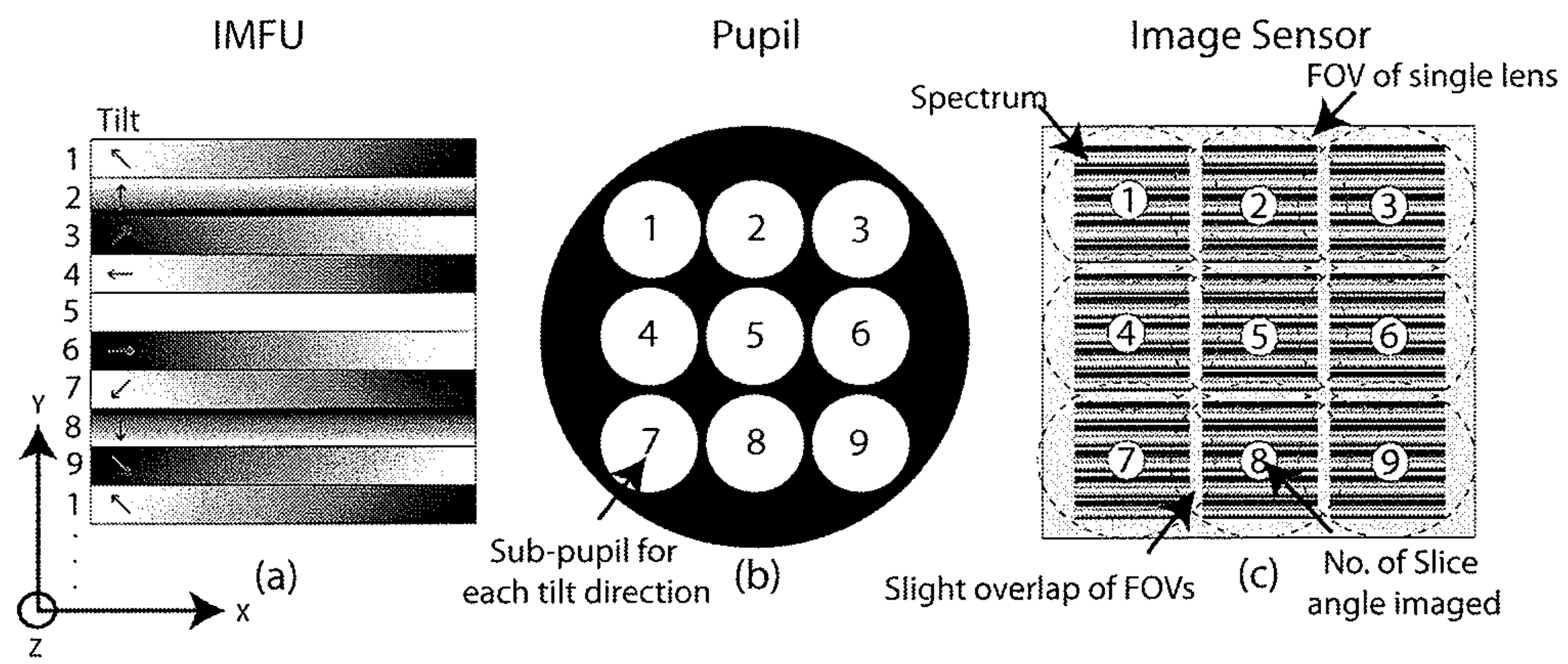


Fig. 13



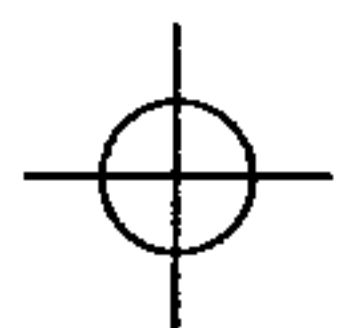


Fig. 14

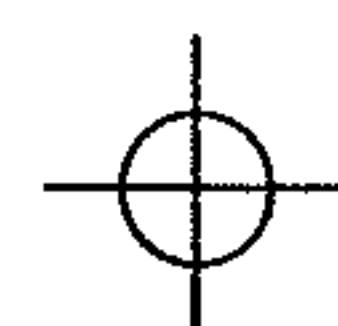
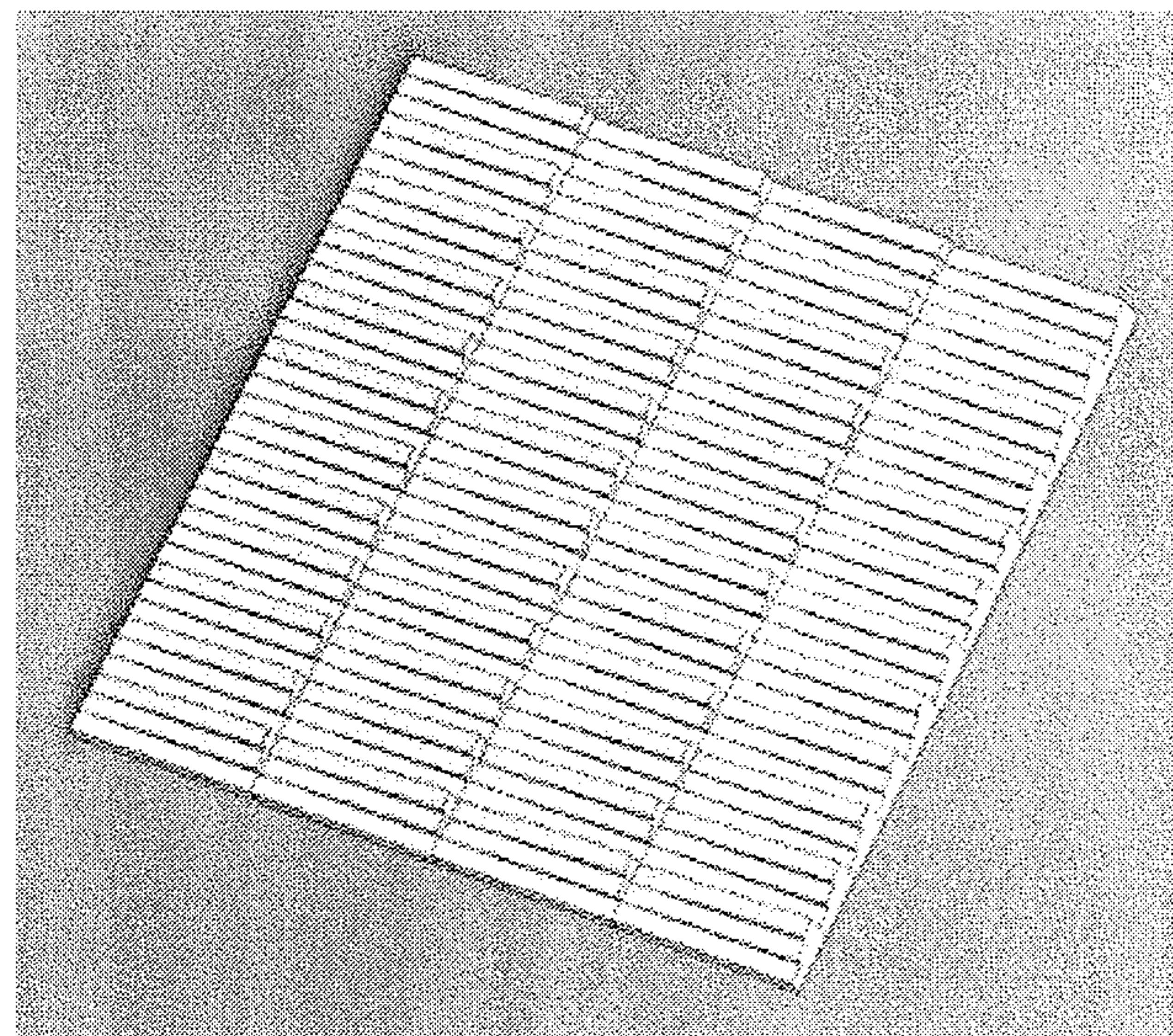
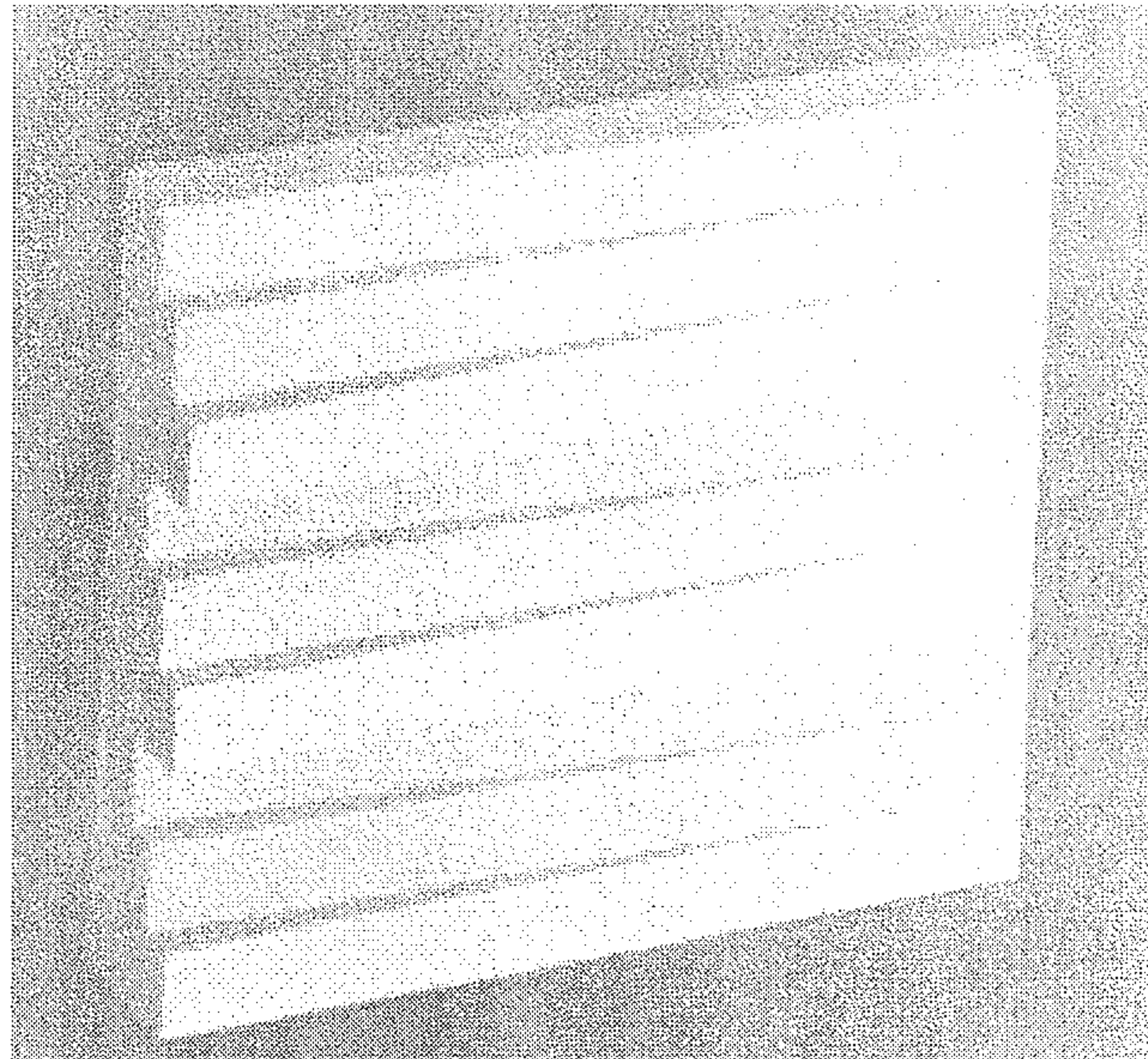


Fig.15

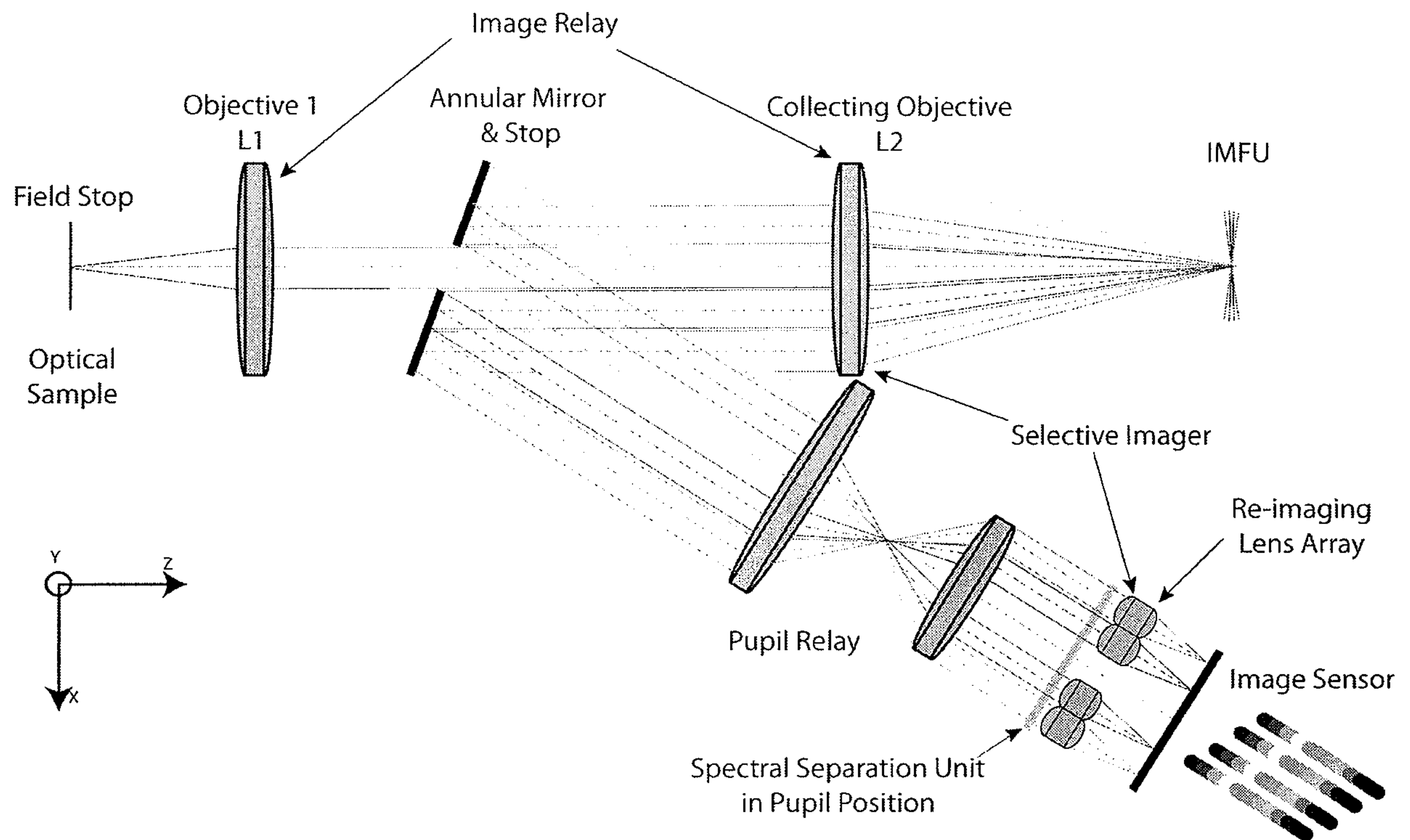


Fig. 16

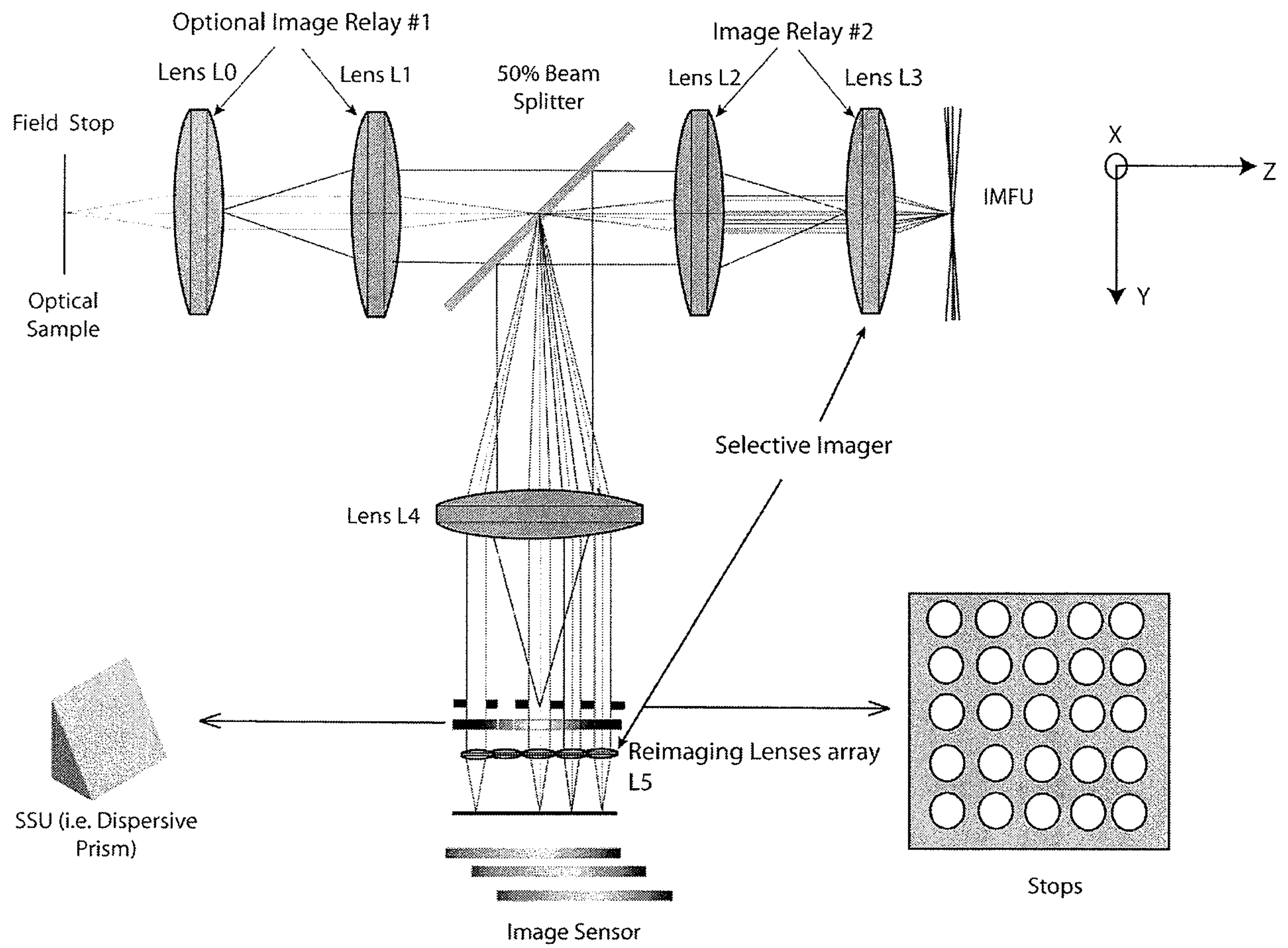


Fig. 17

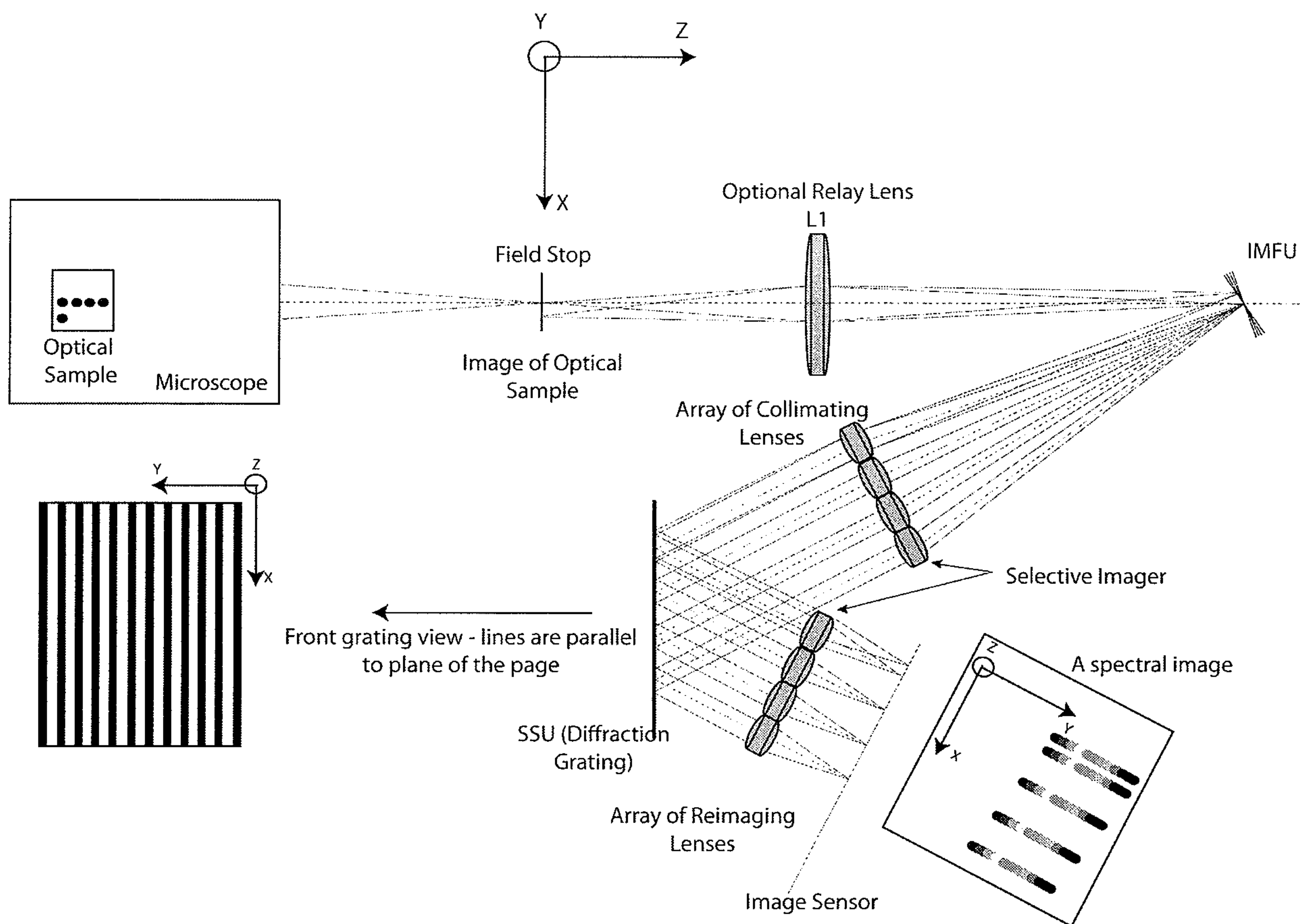
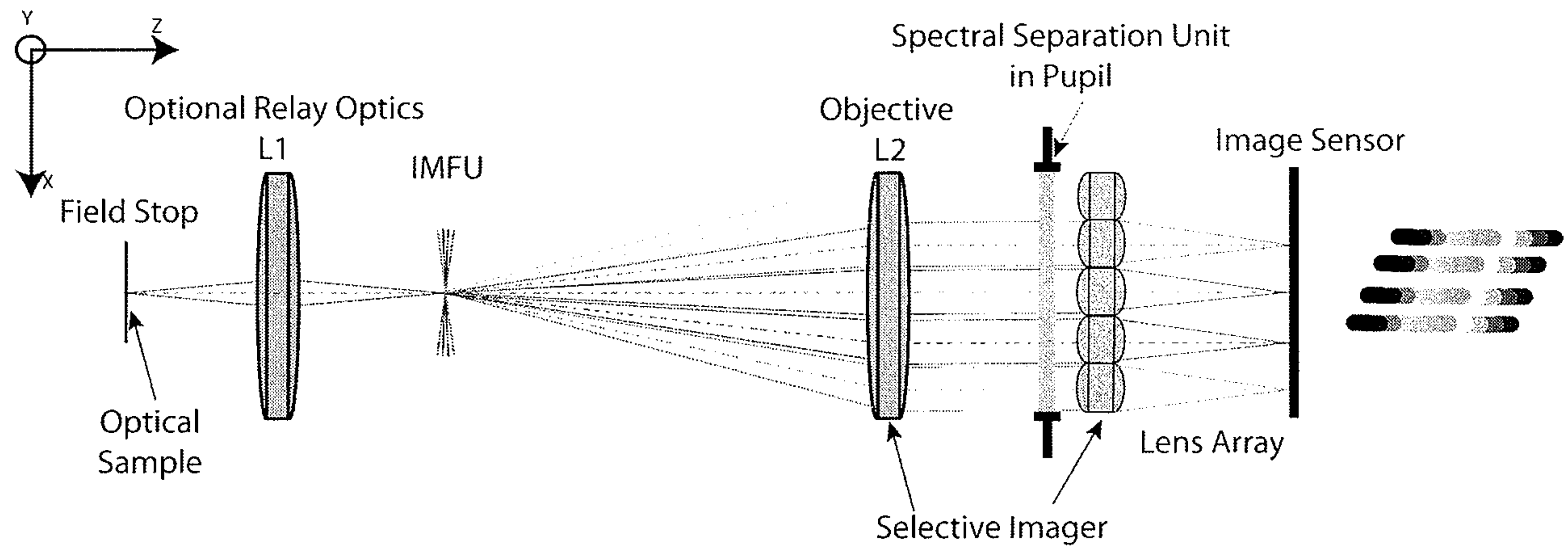


Fig. 18



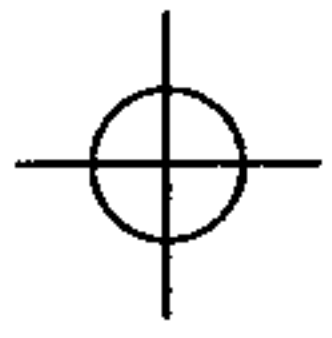
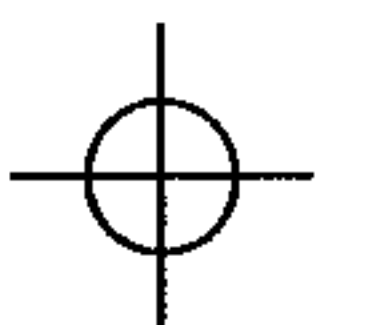
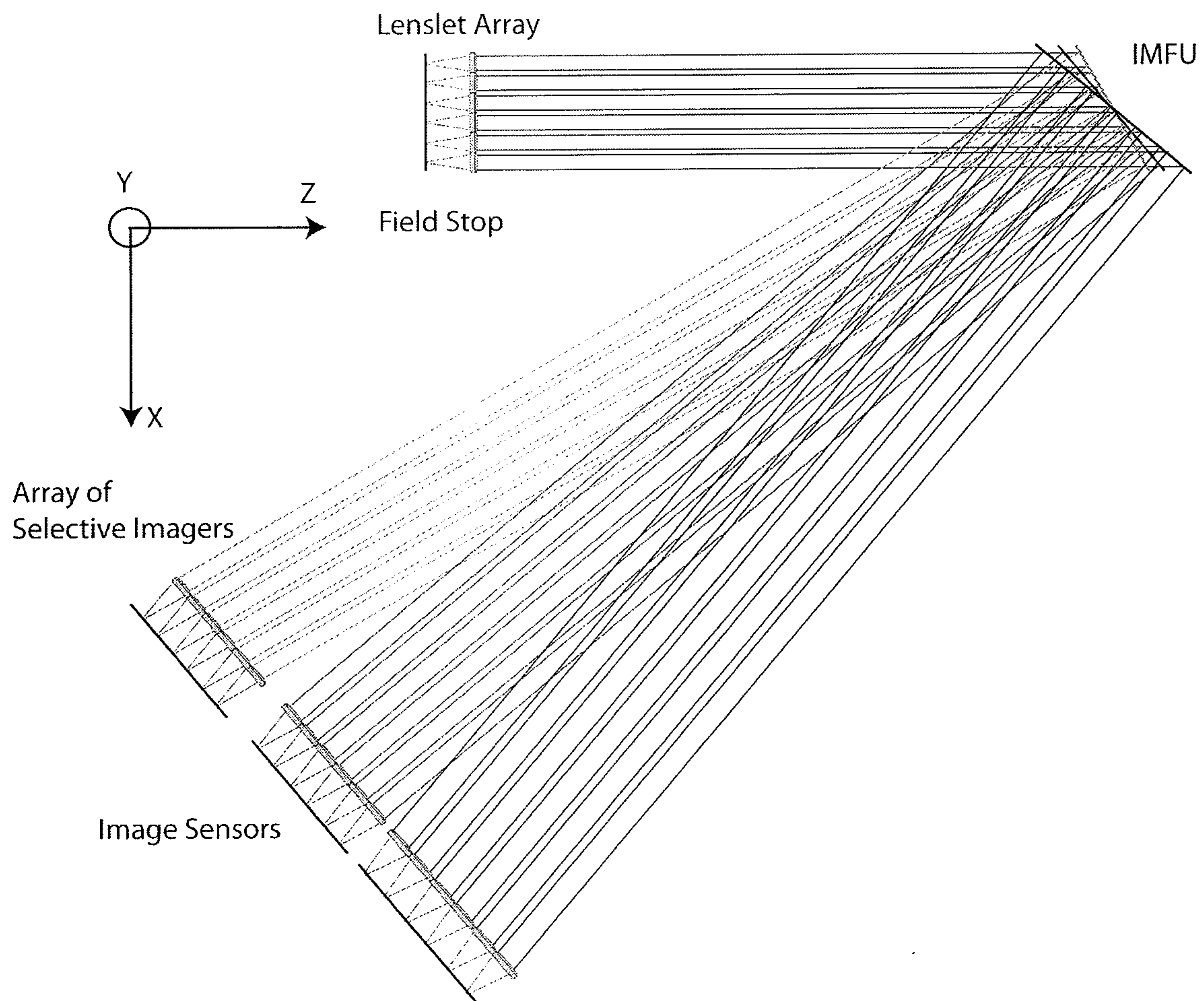


Fig. 19



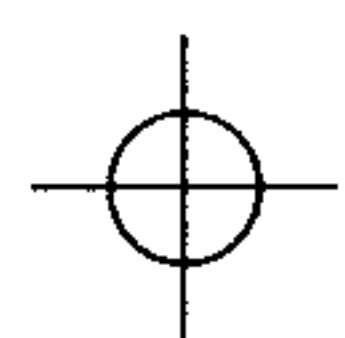
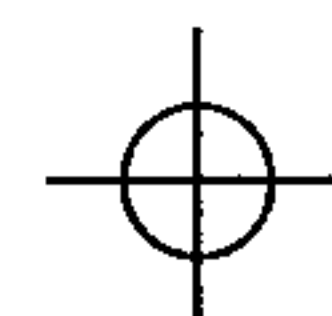
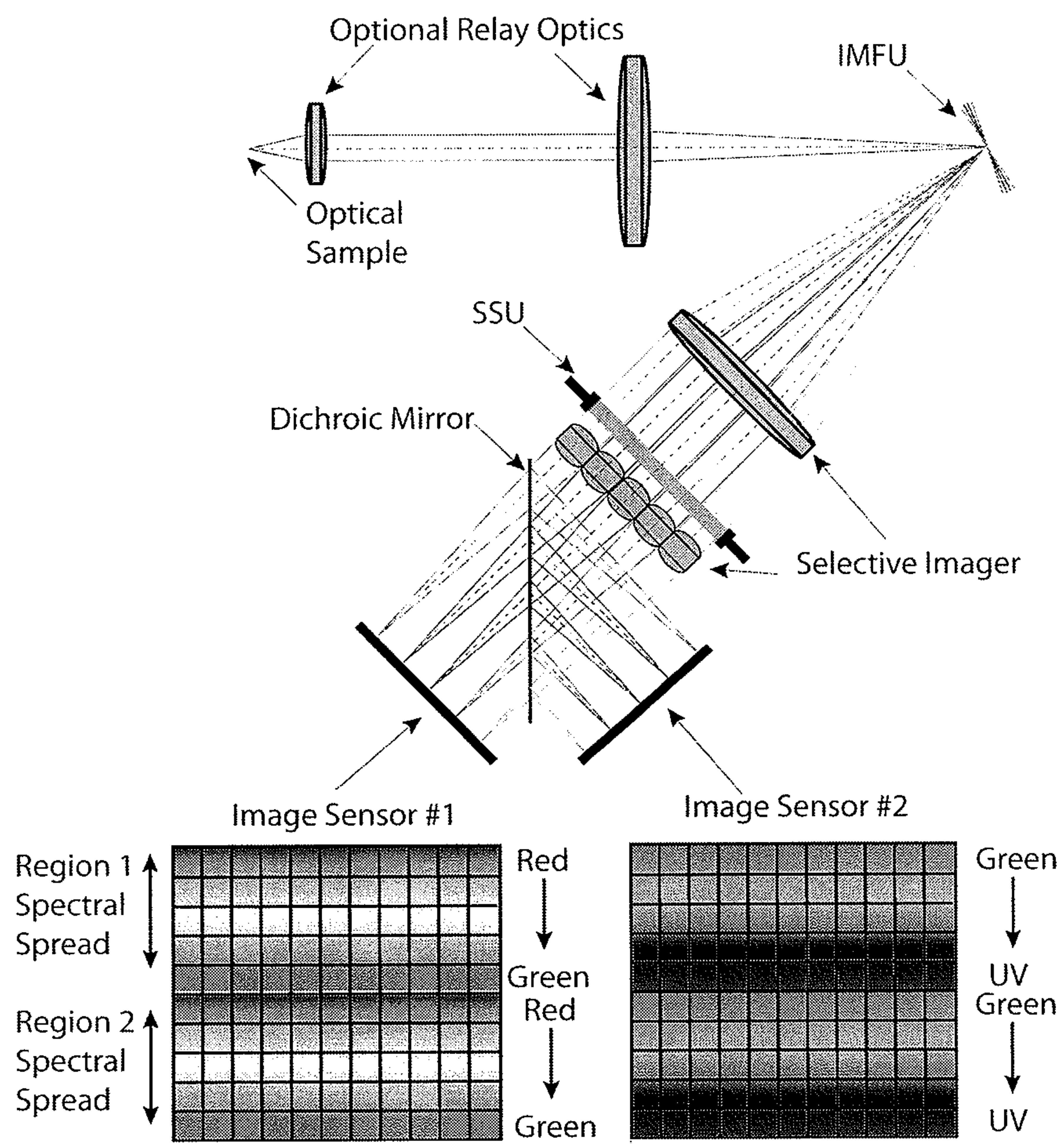


Fig. 20



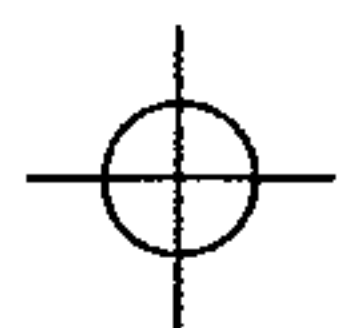
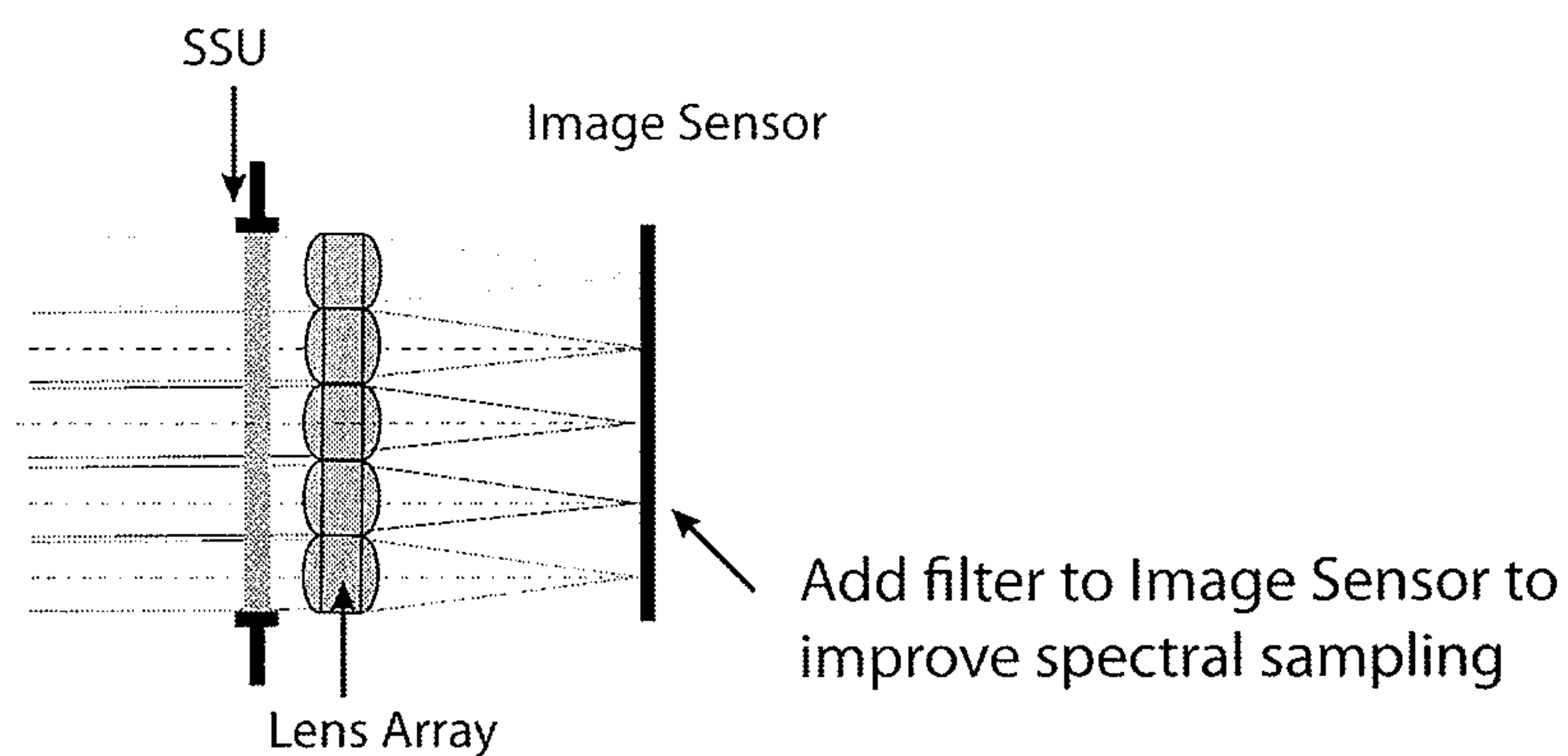
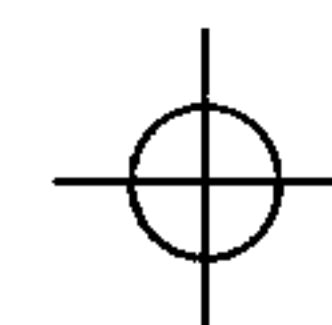
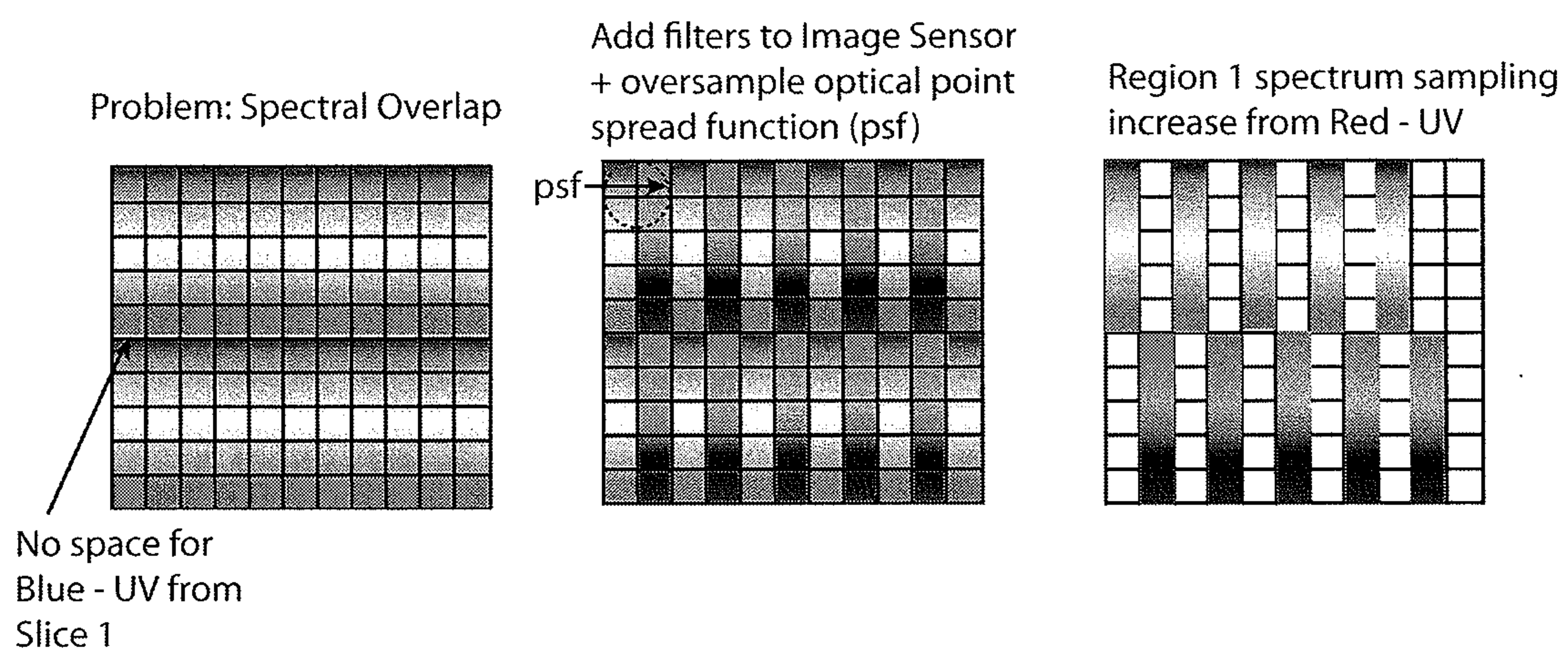


Fig. 21



Example: Spectral Filters on Image Sensor



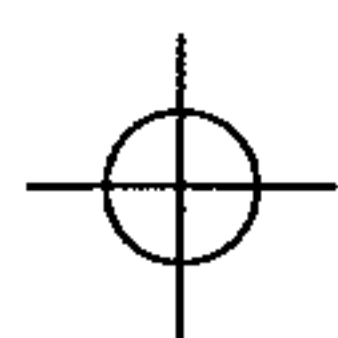
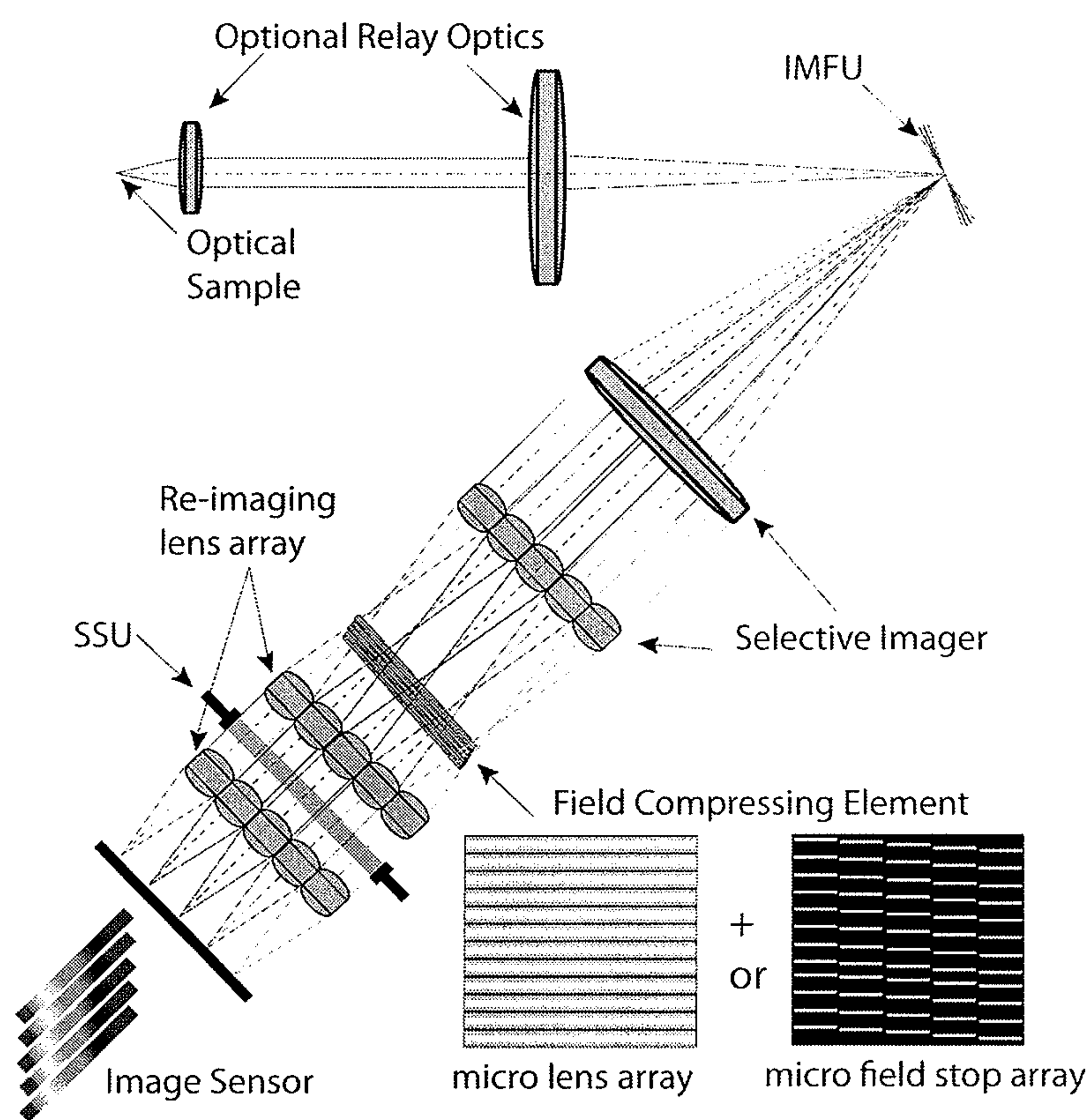


Fig. 22



Single Slice Optical Path from Selective Imager

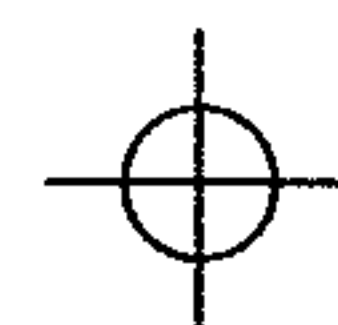
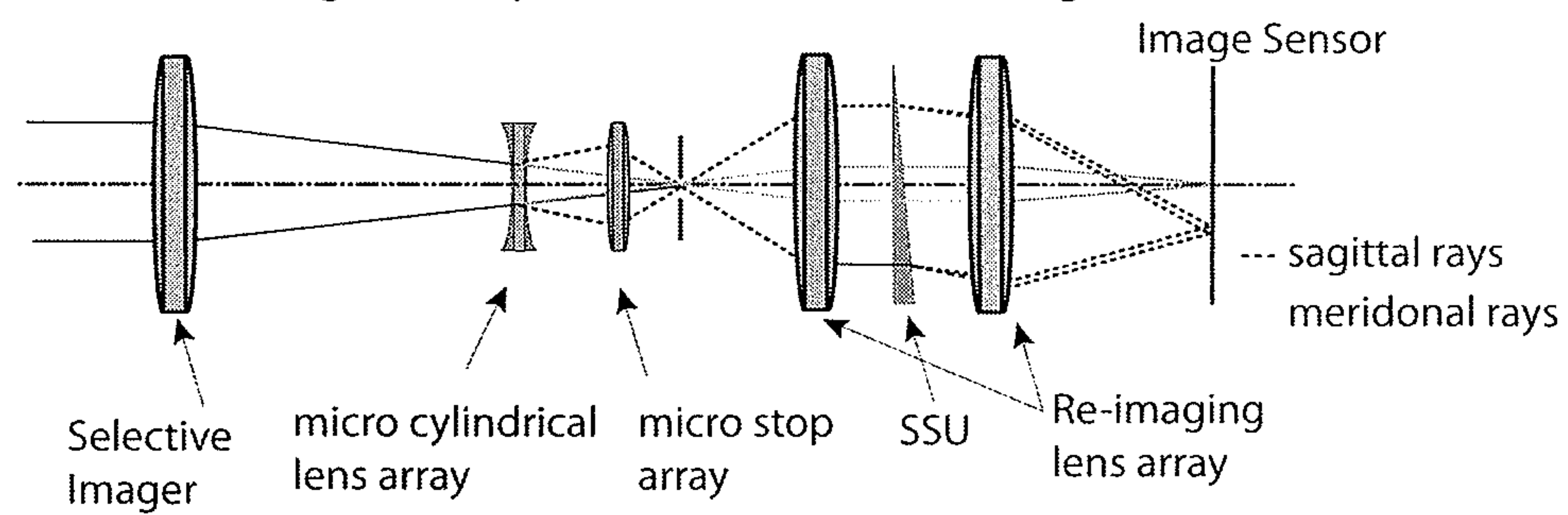
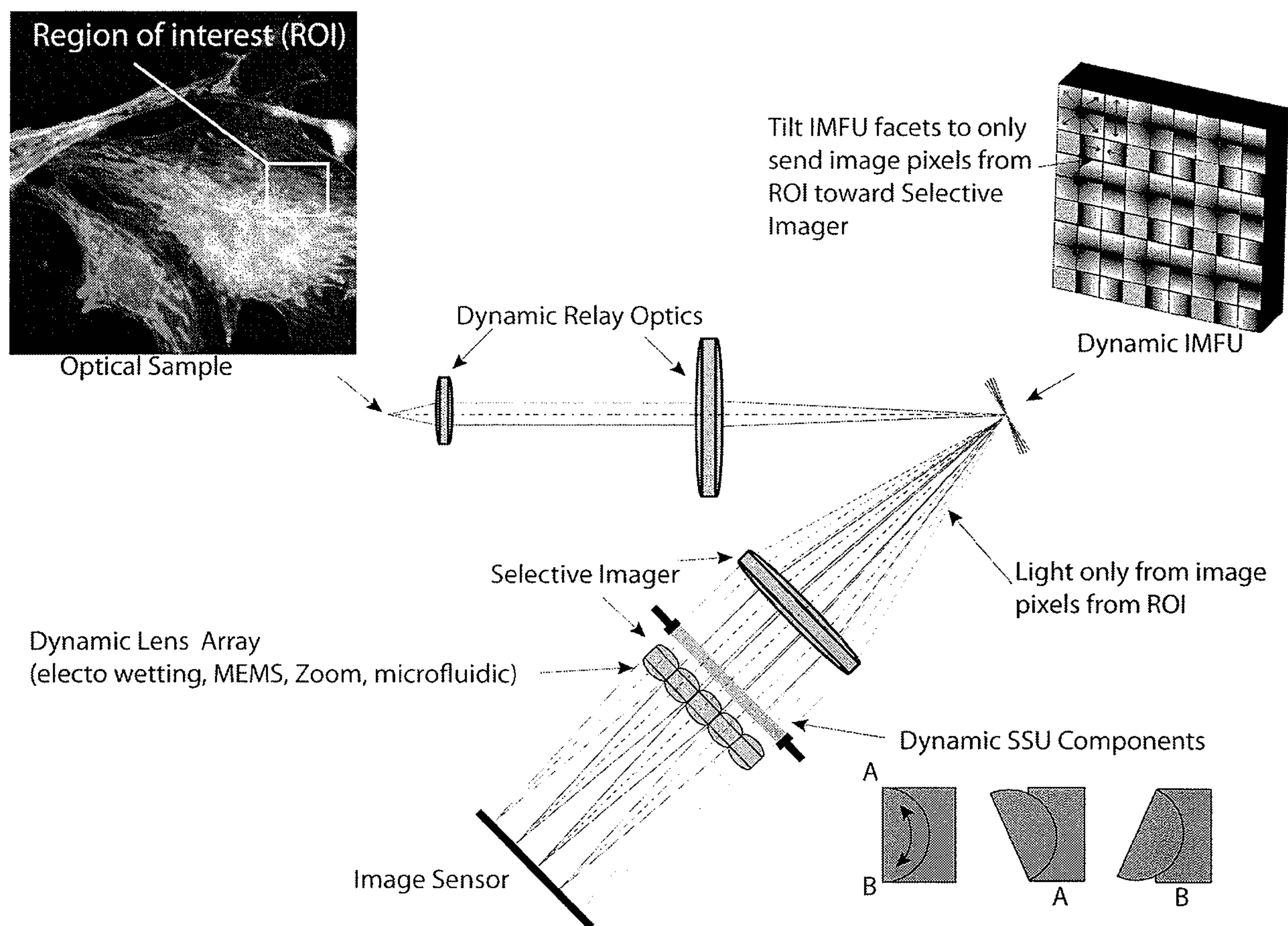


Fig. 23



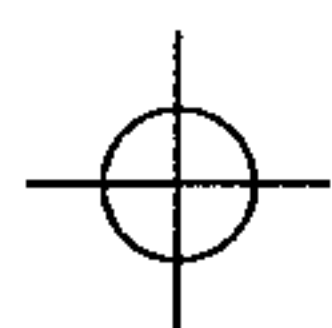
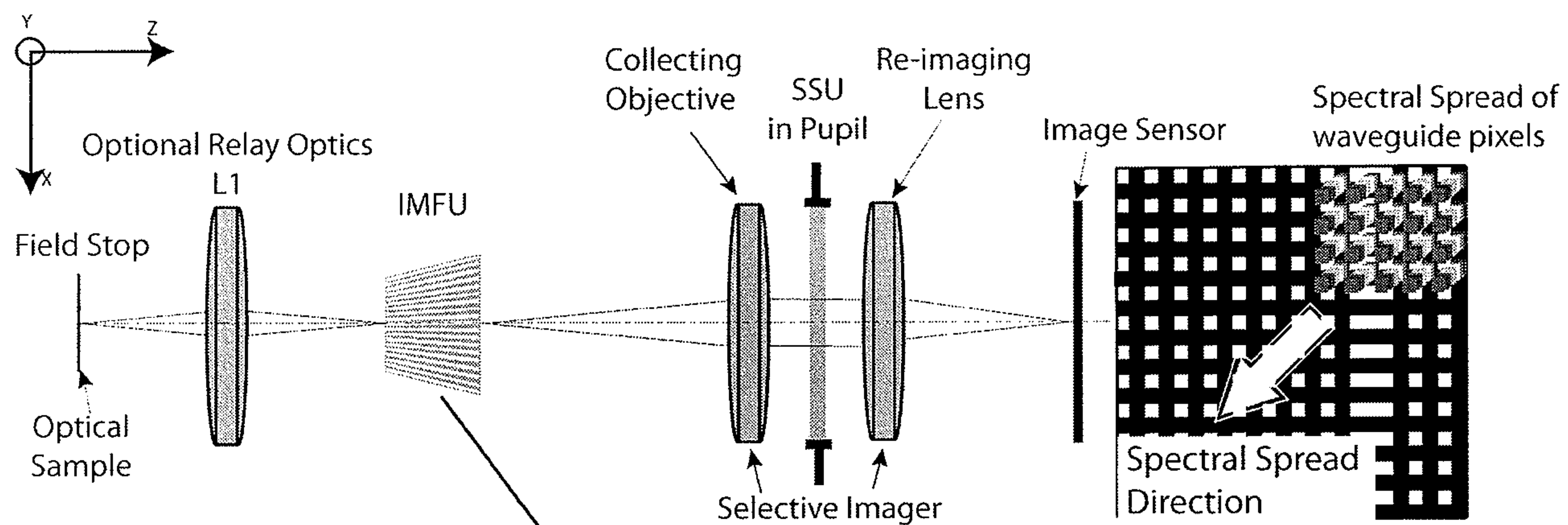
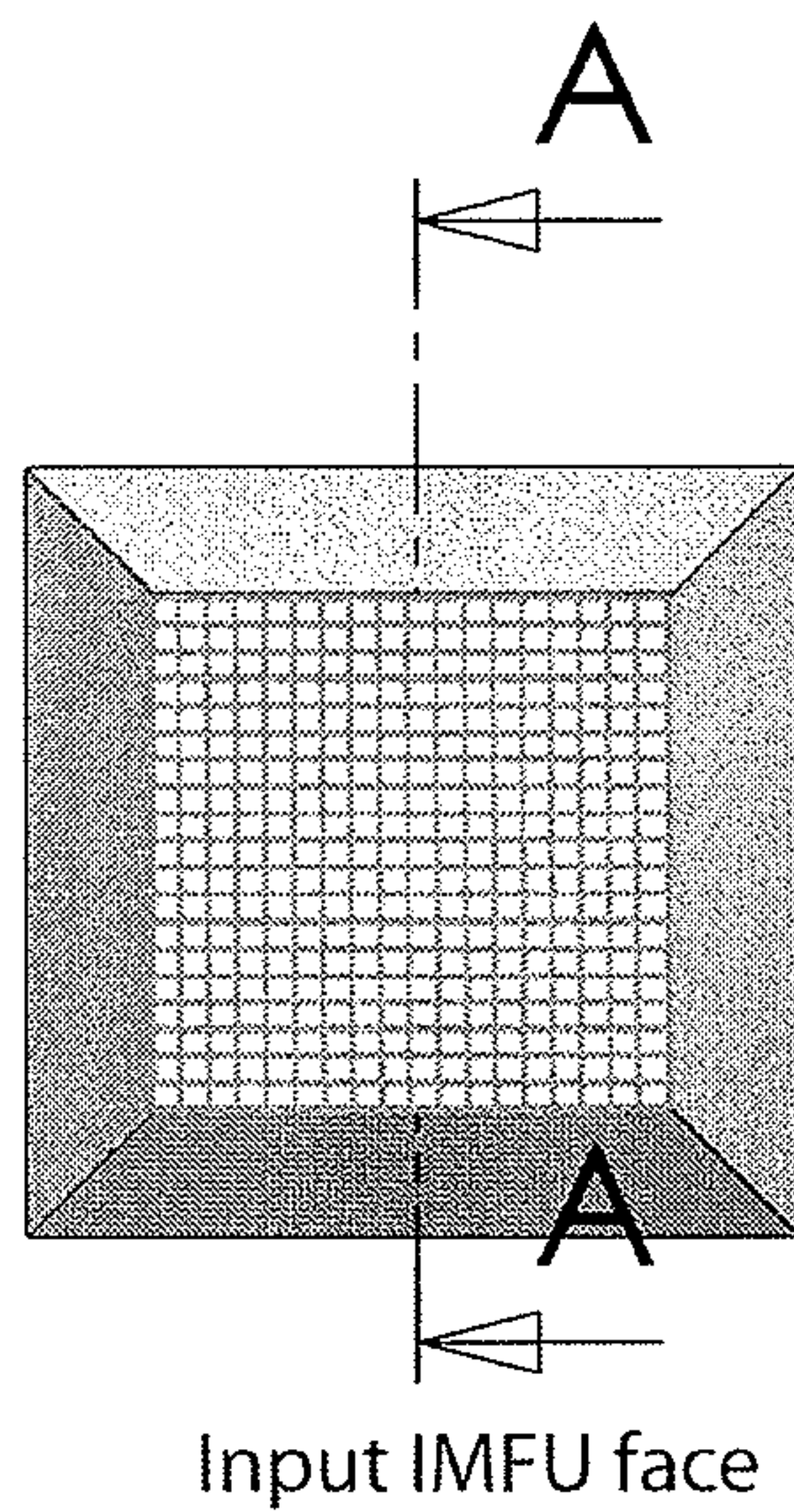
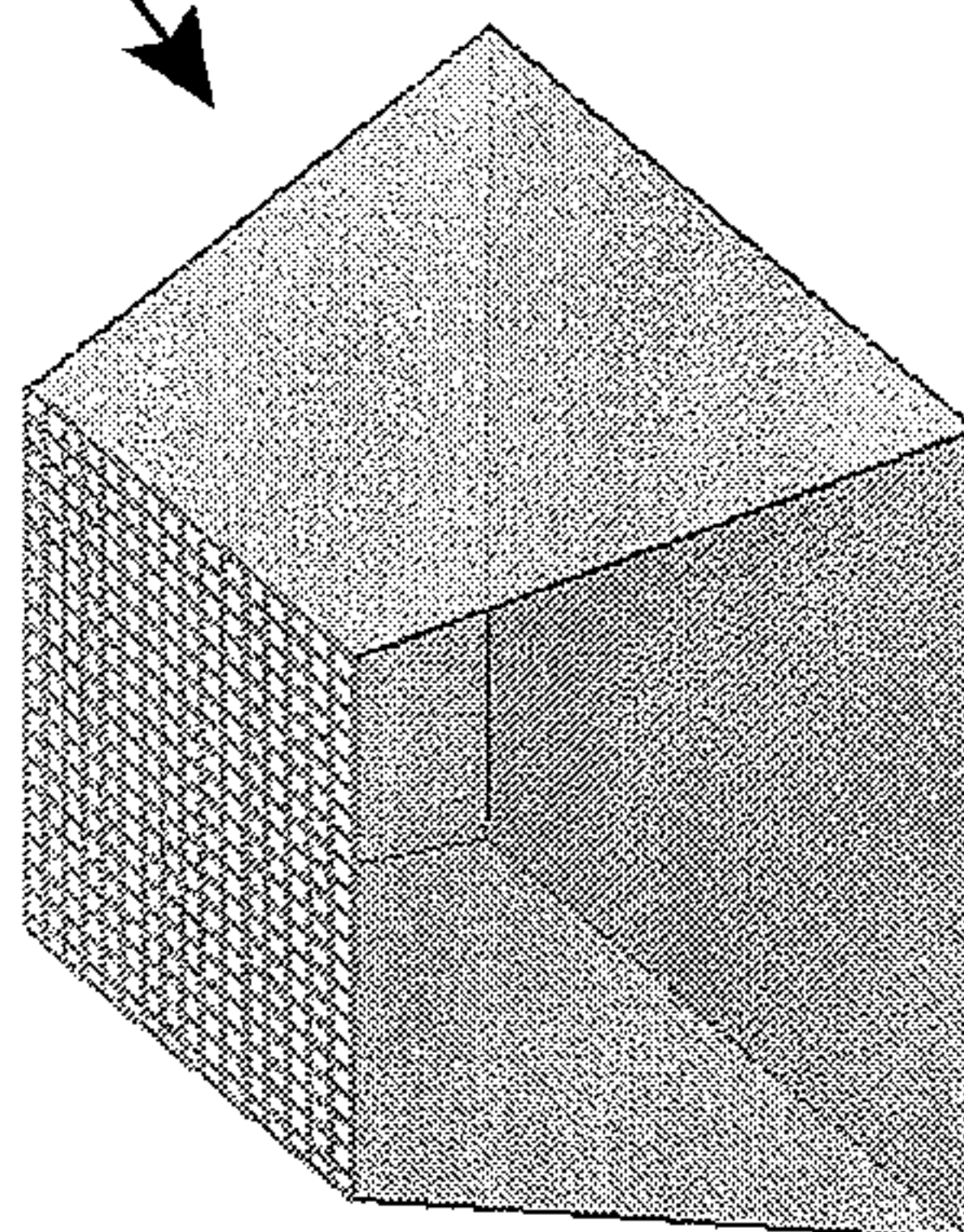


Fig. 24

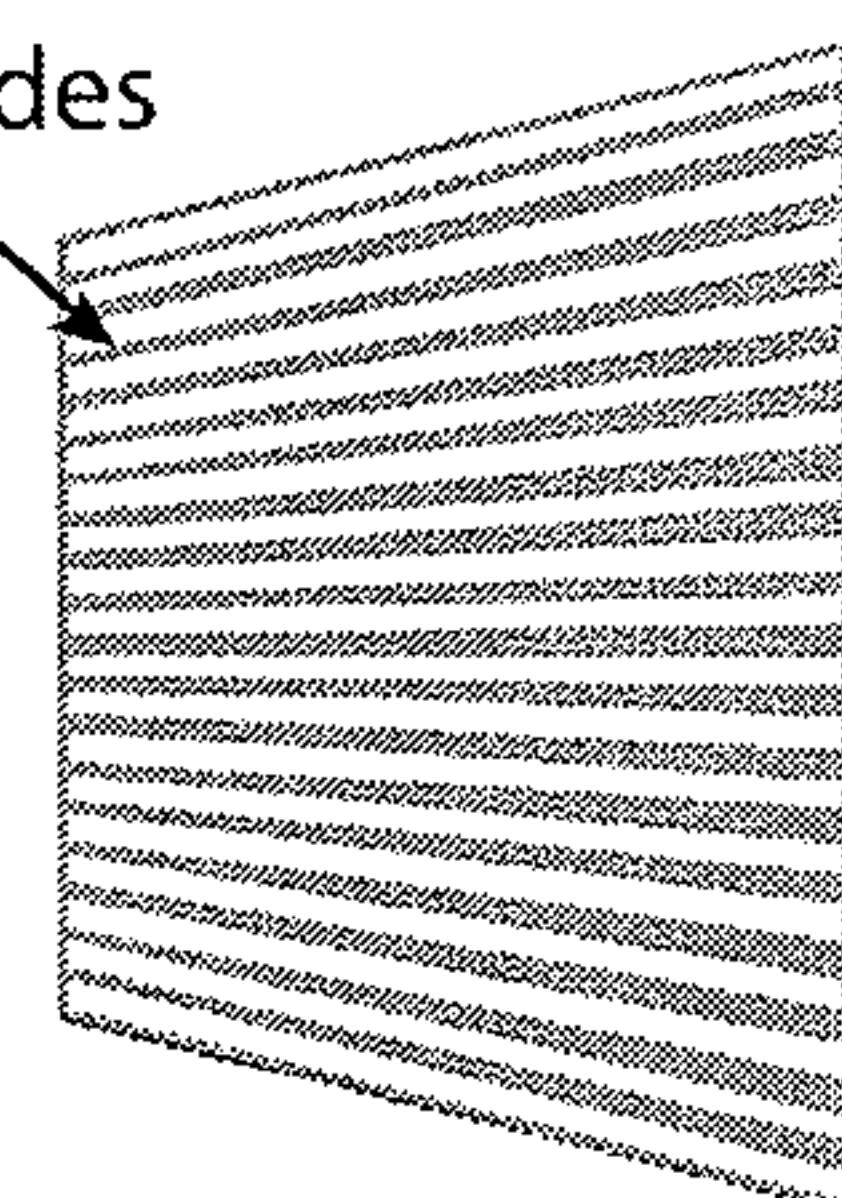


(a) Waveguide IMS layout

Isometric View

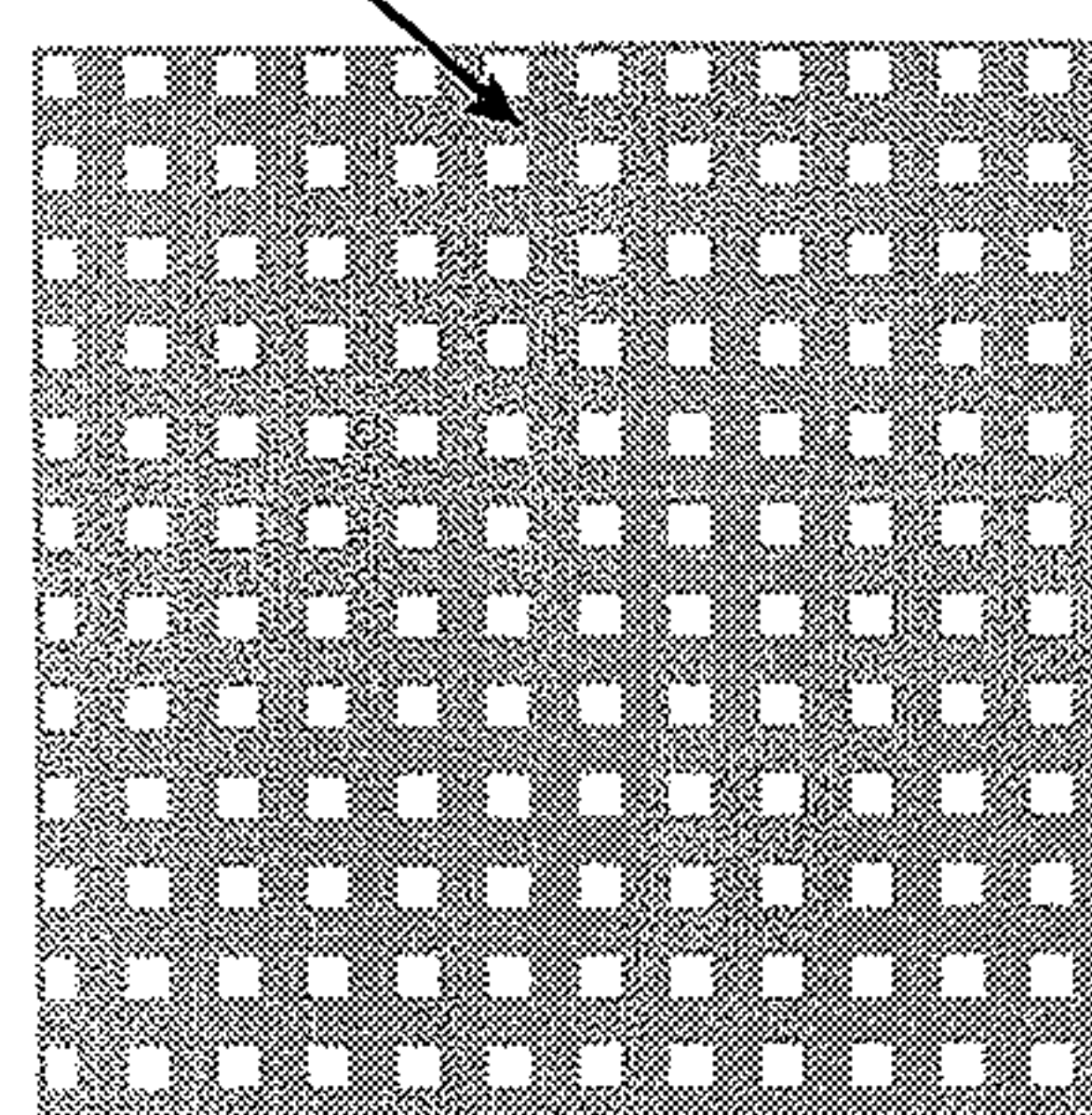


Individual wave guides



Cross Section (A)

Space between individual waveguides can be filled with its spectral content .



Output IMFU face

(b) Waveguide Mapper Concept

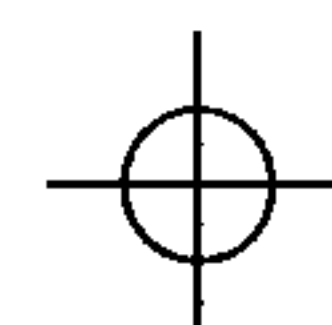
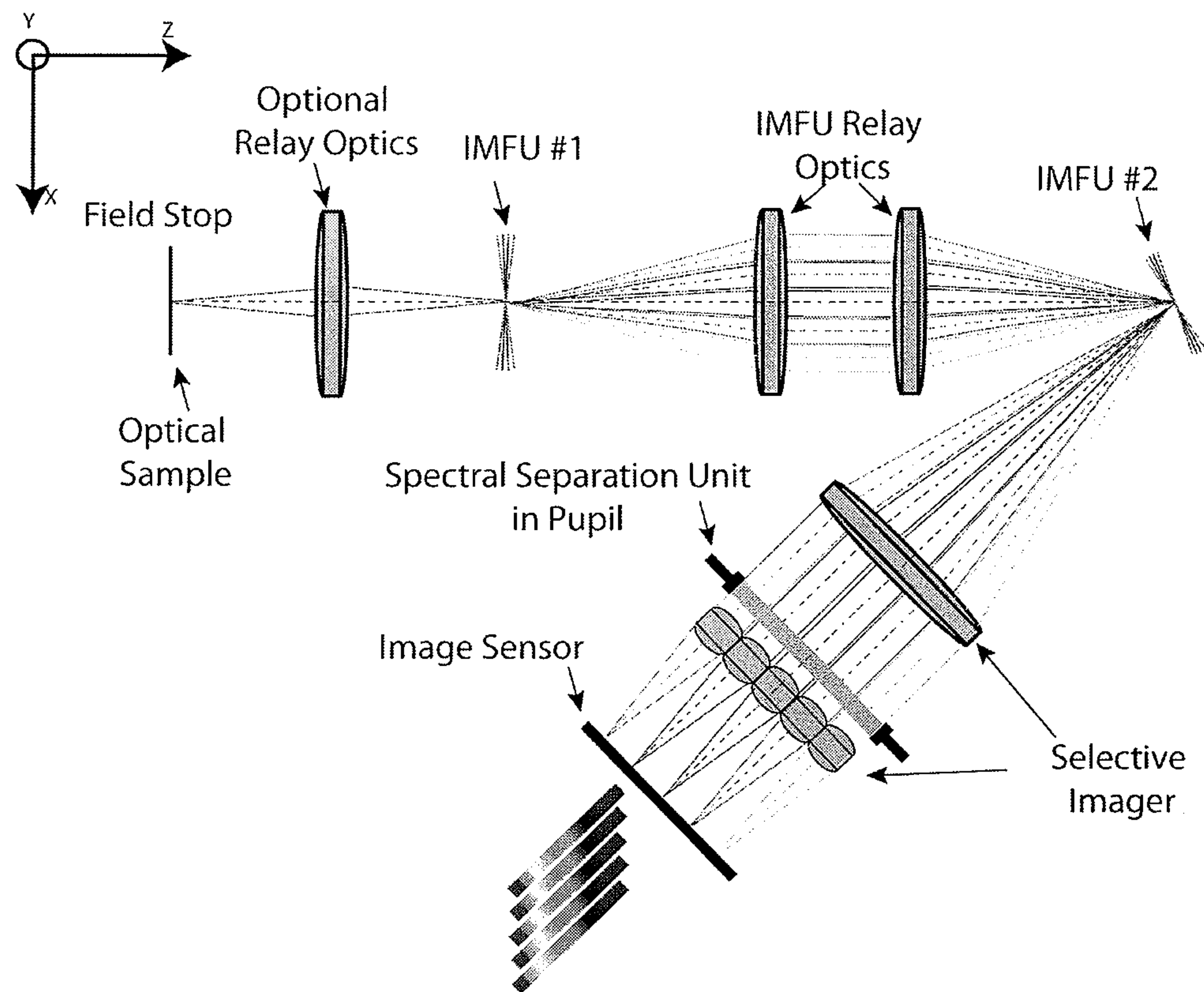


Fig. 25



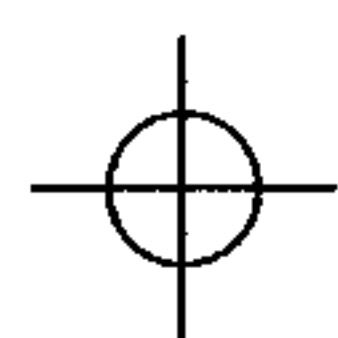
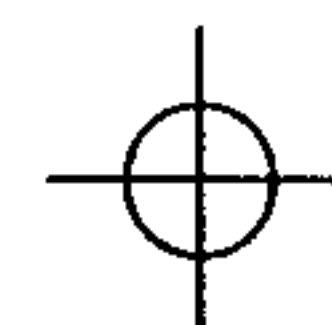
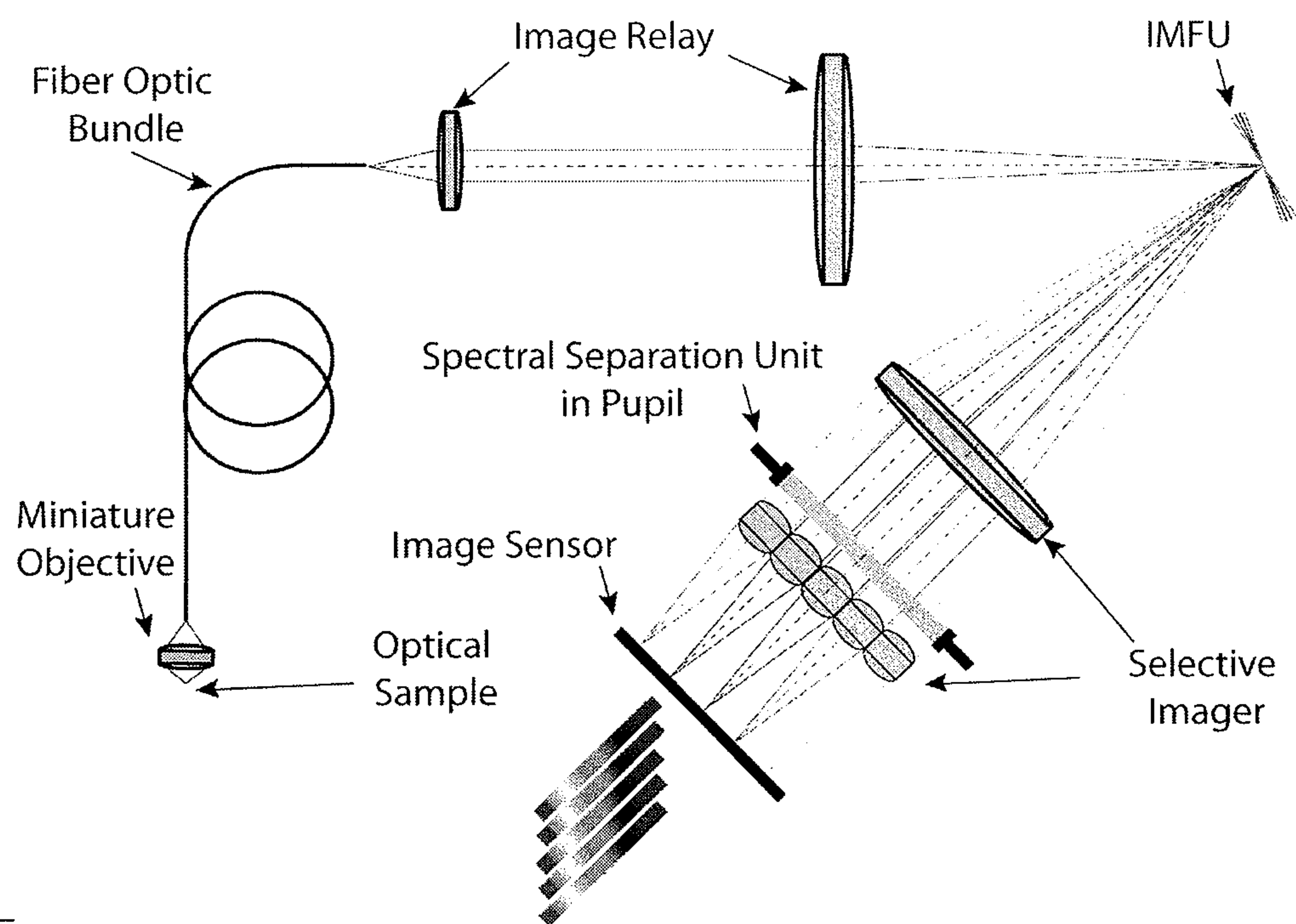


Fig. 26



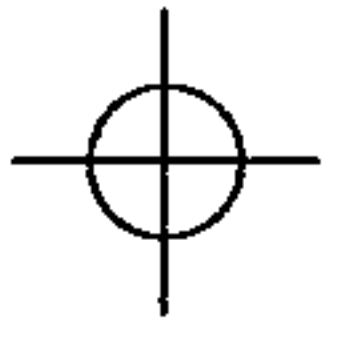
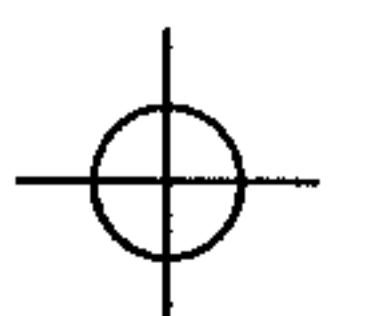
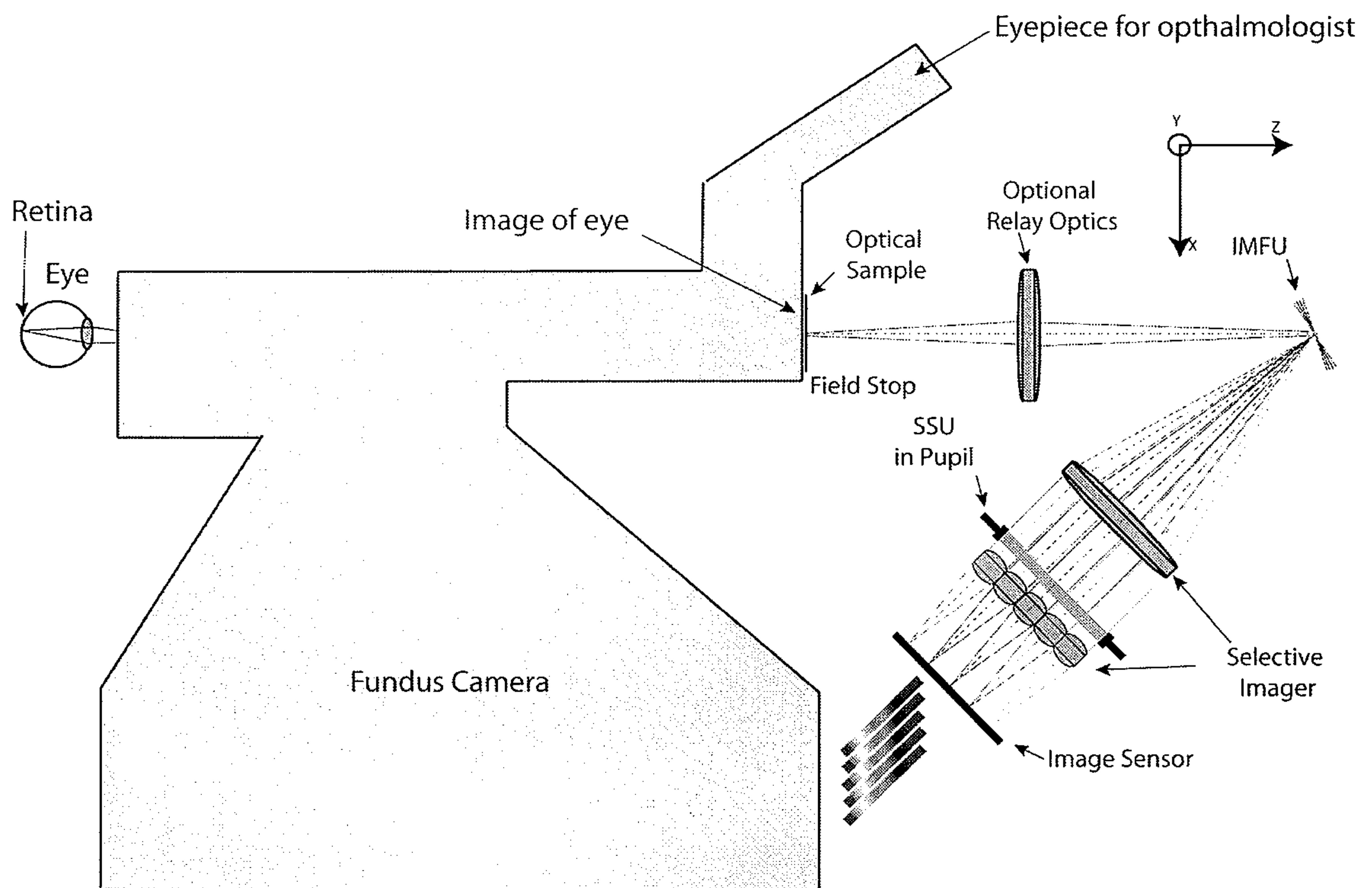


Fig. 27



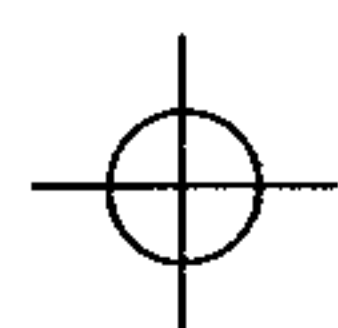


Fig. 28

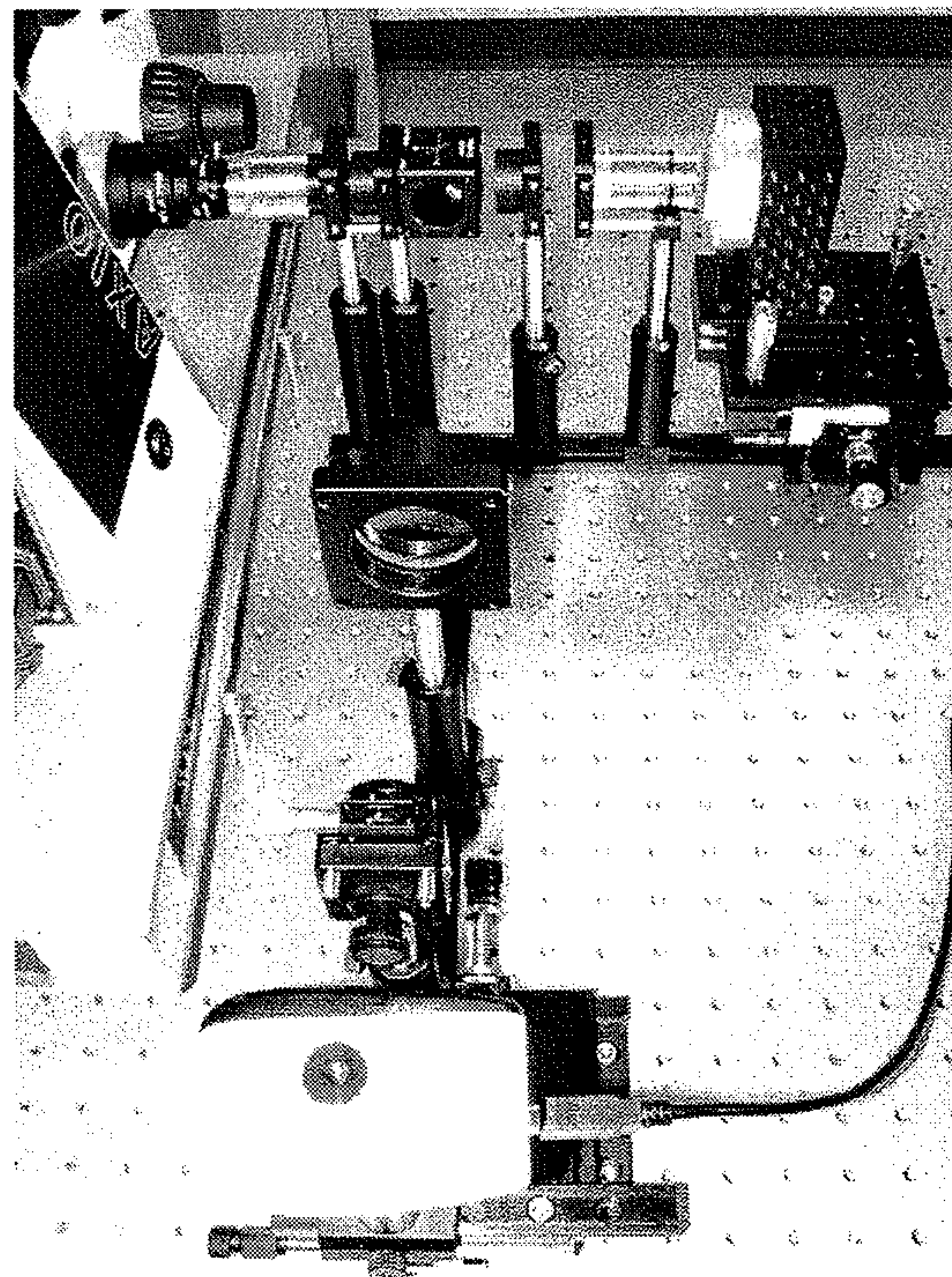
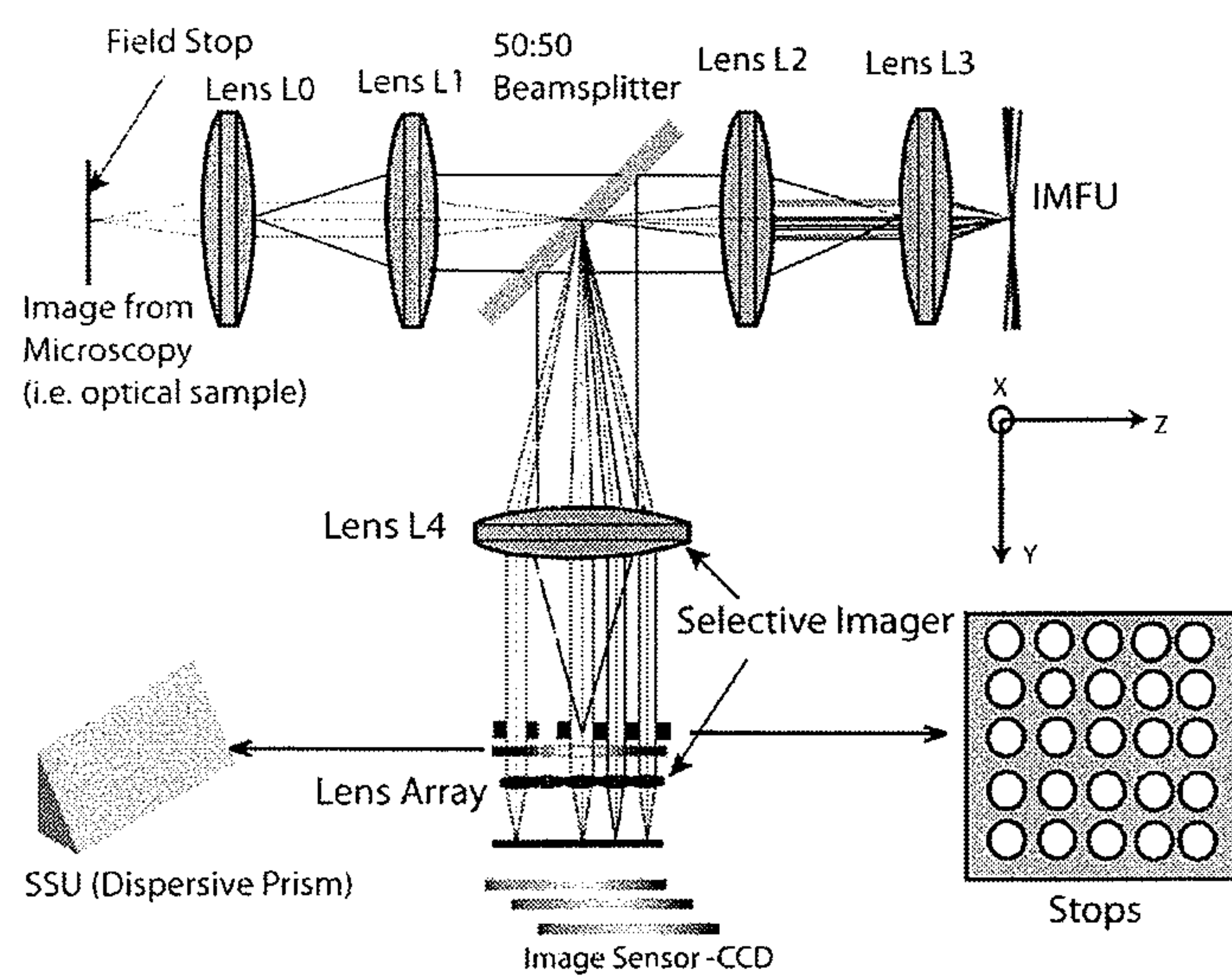
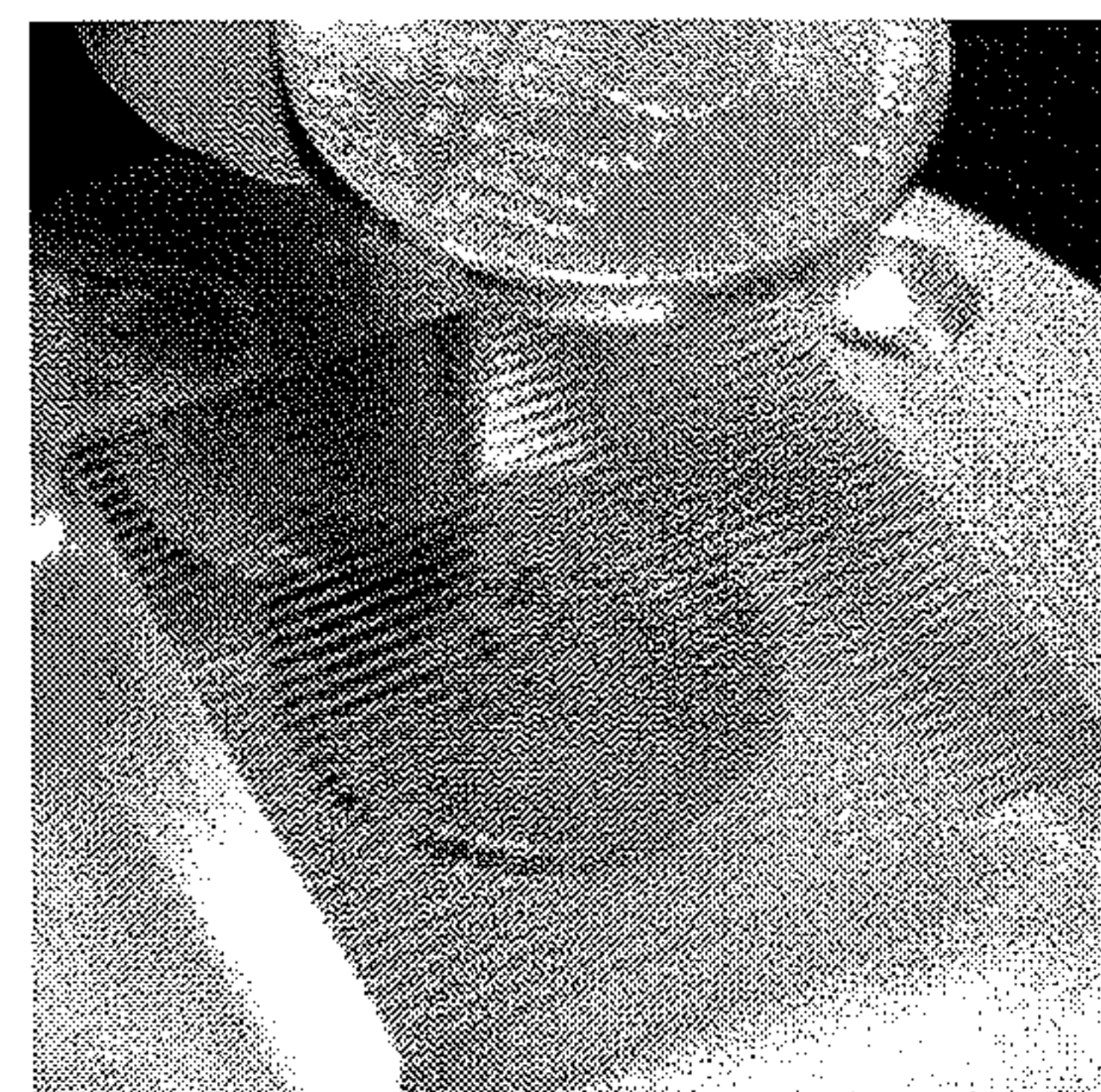


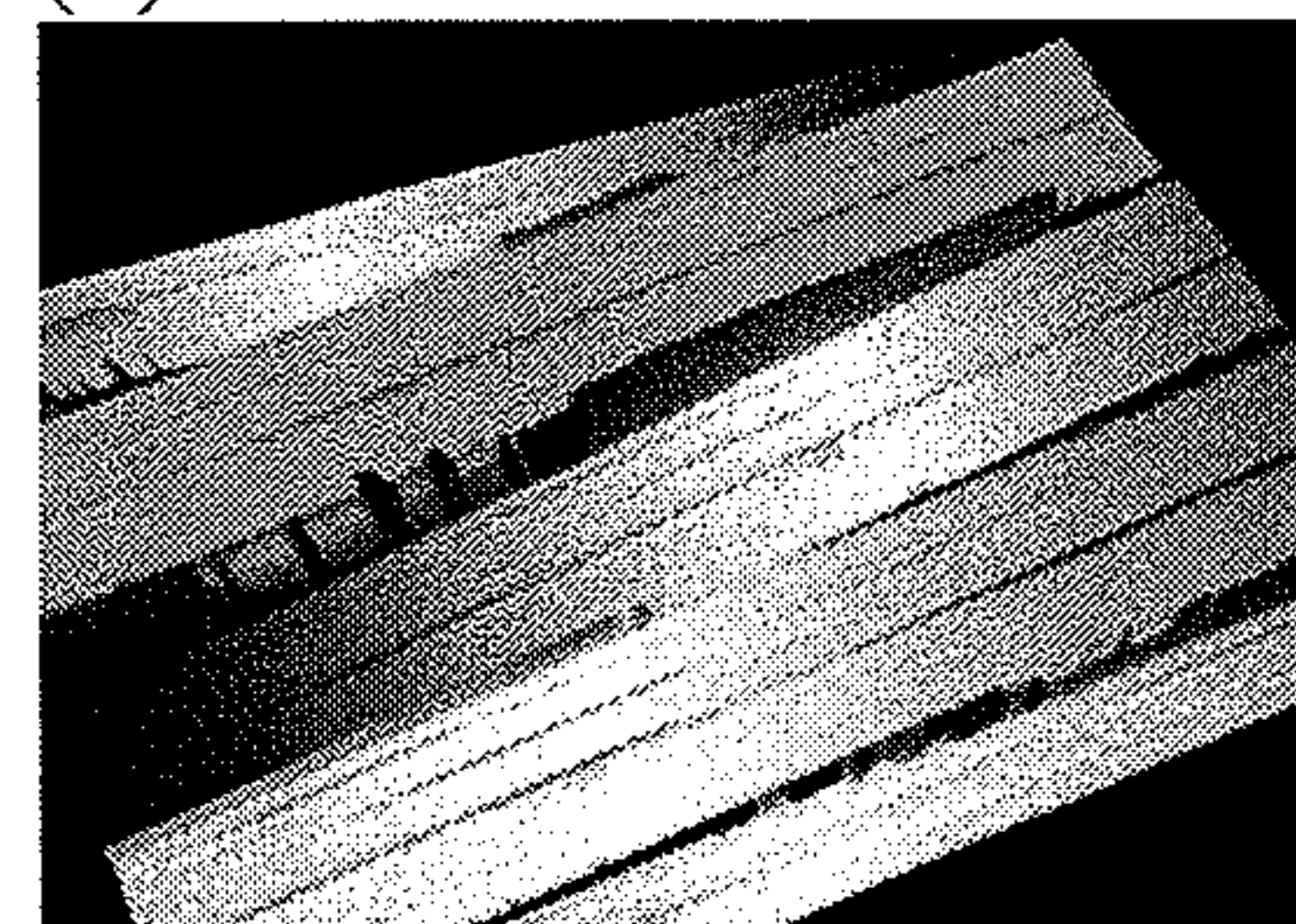
Fig. 29



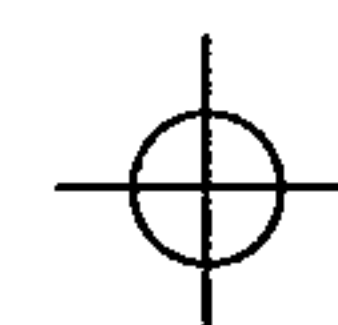
(a)



(b)



(c)



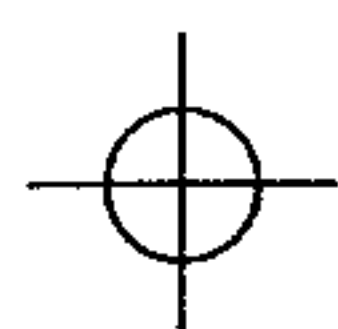
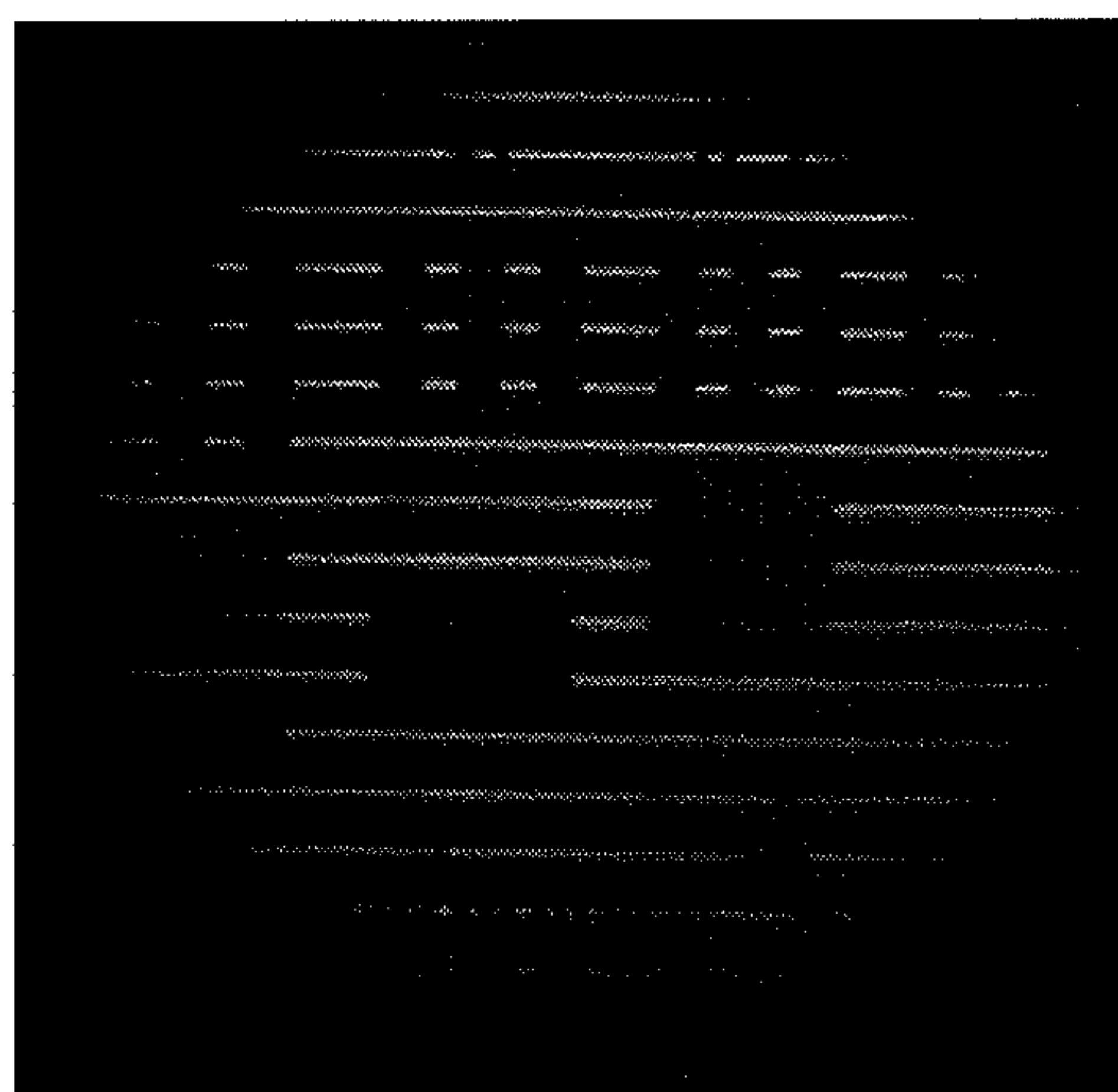
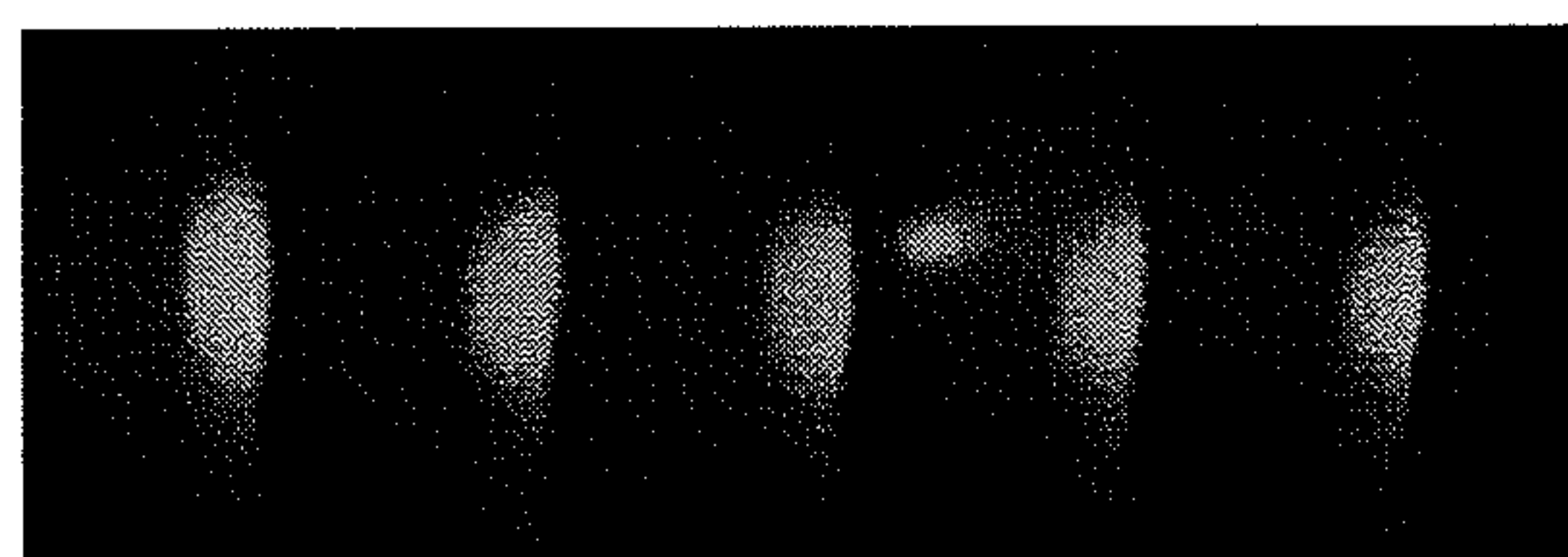


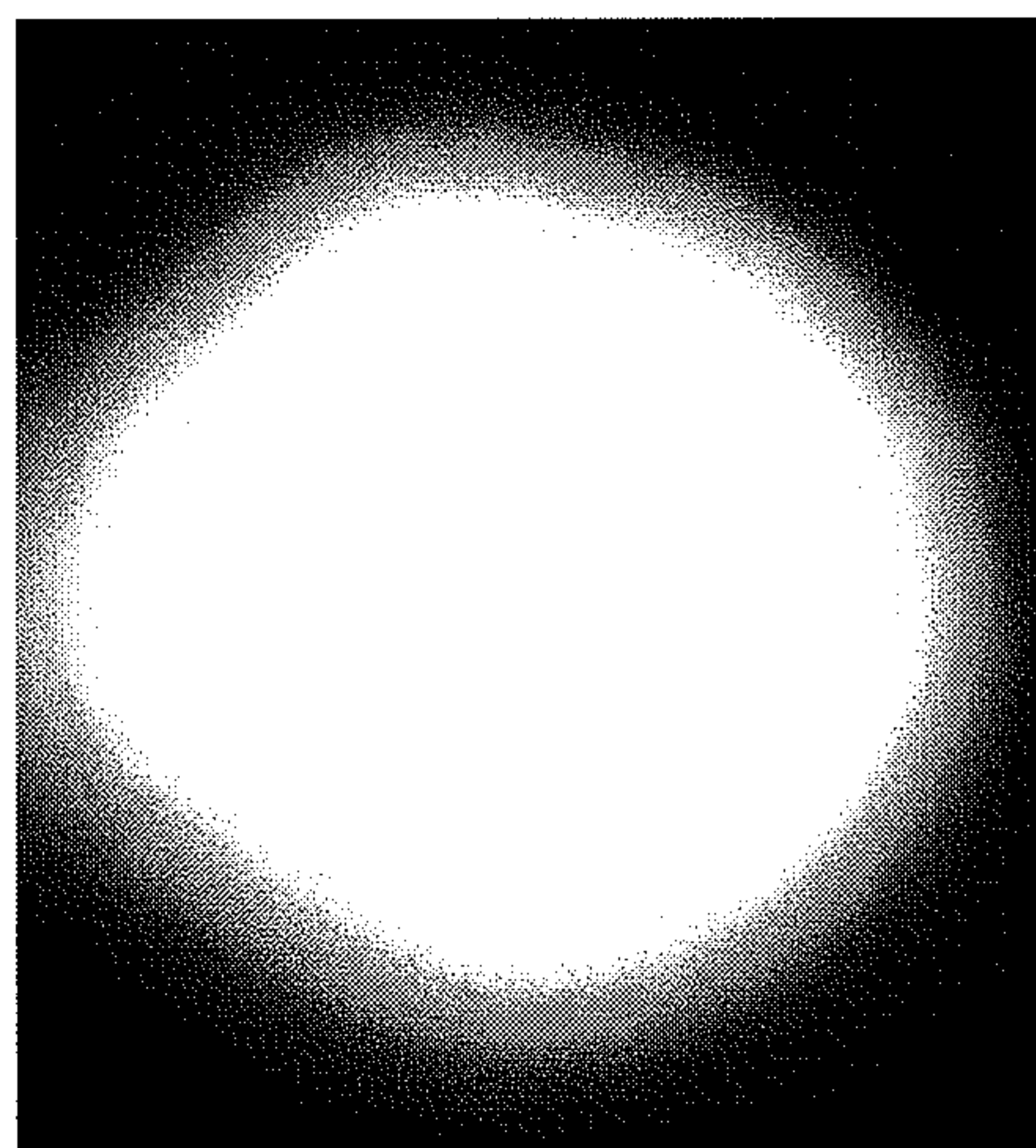
Fig. 30



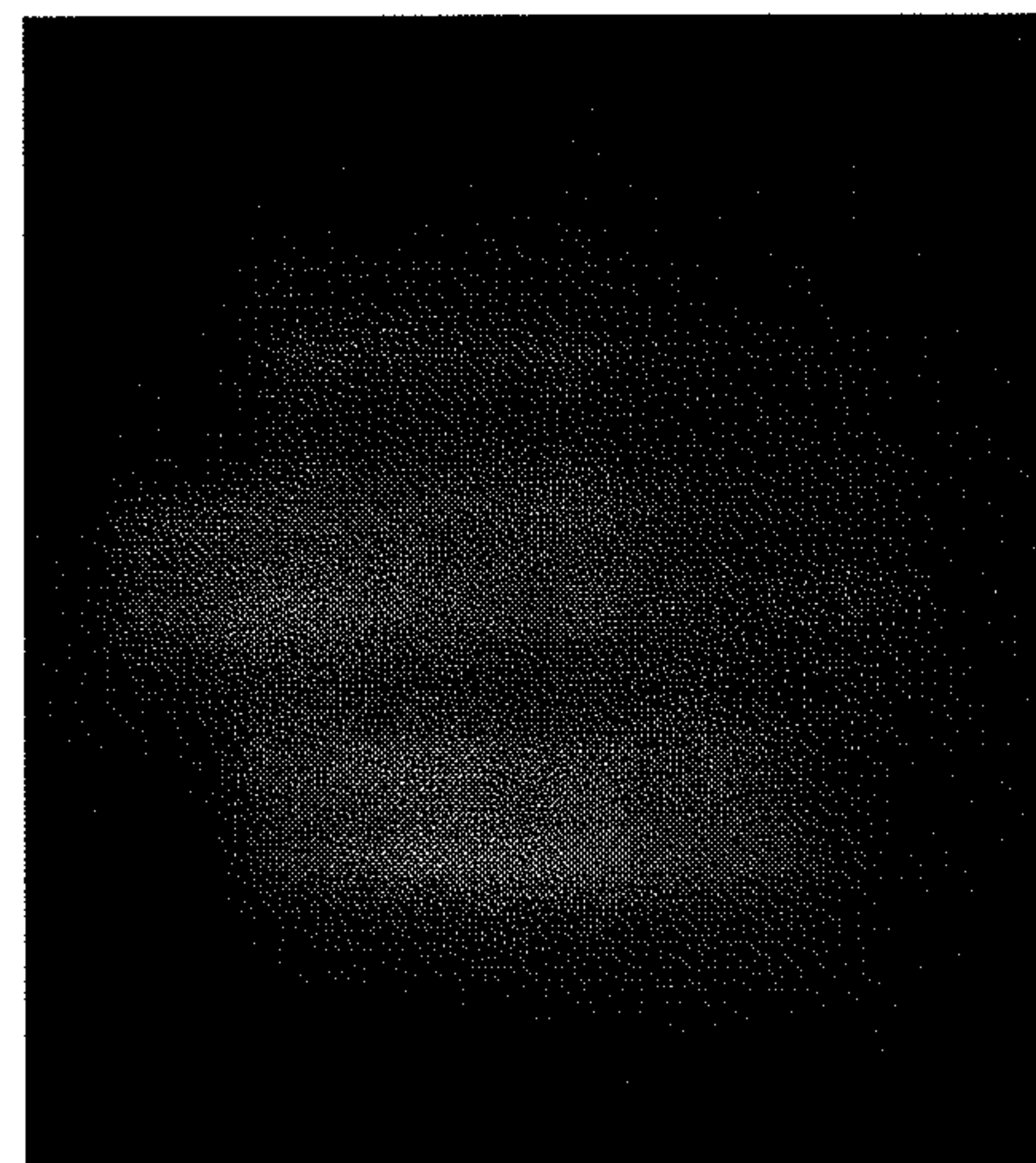
(a)



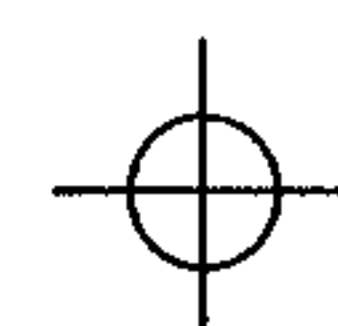
(b)



(c)



(d)



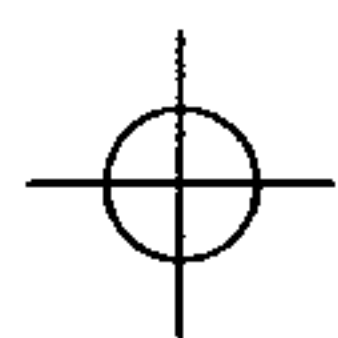
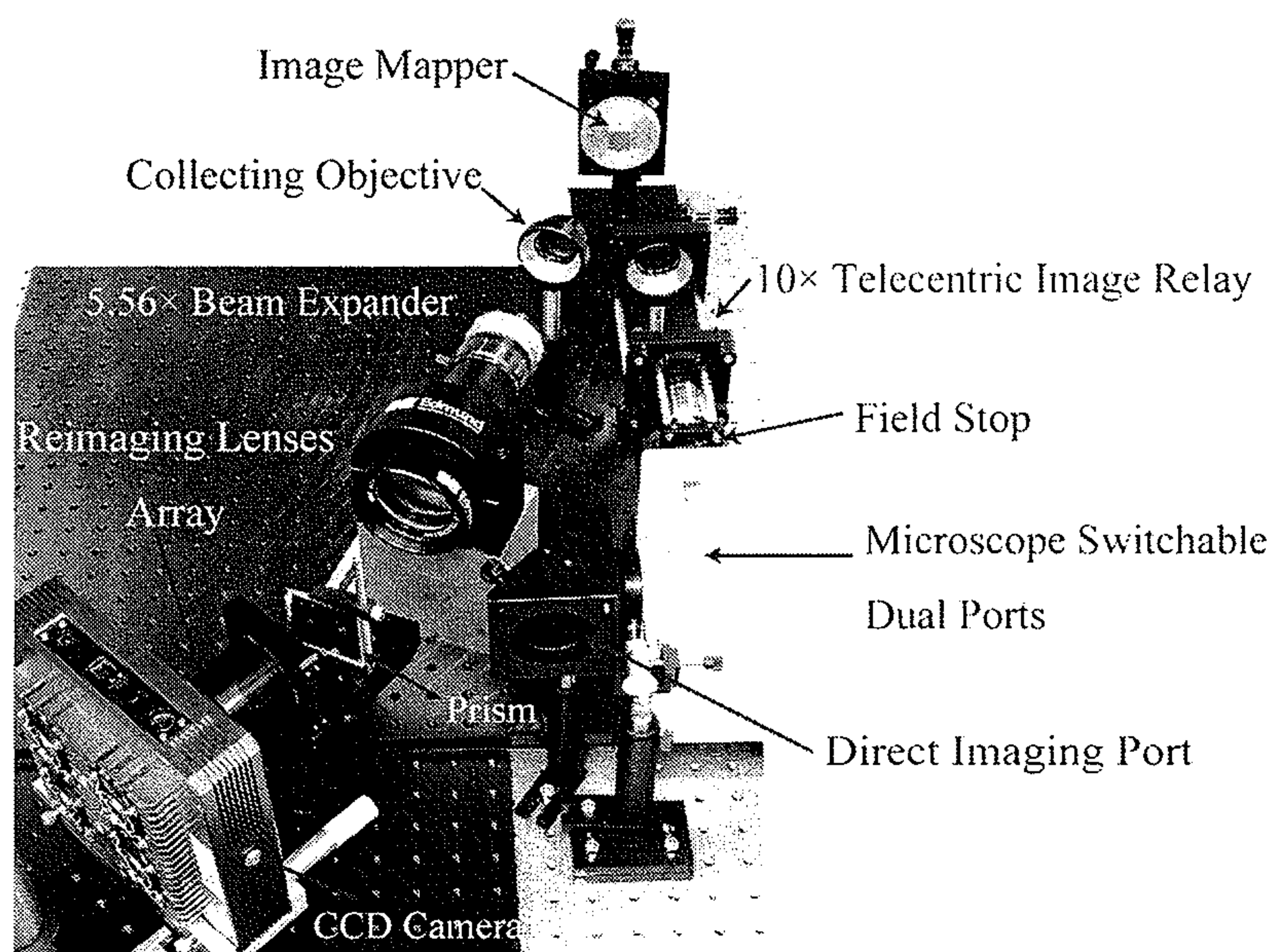
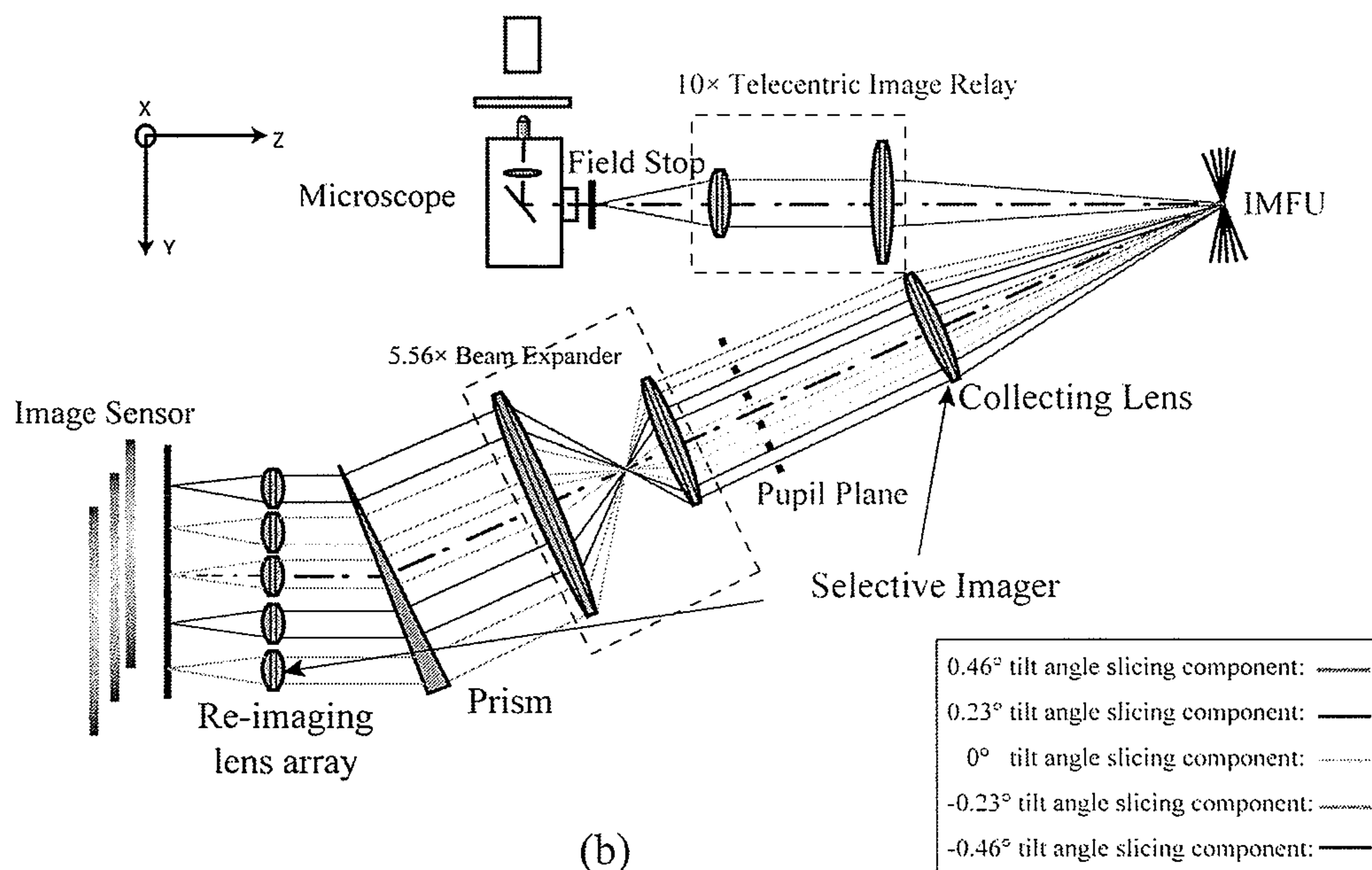


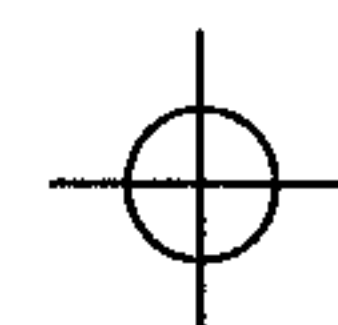
Fig.31



(a)



(b)



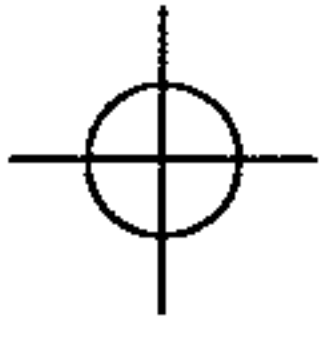


Fig. 32

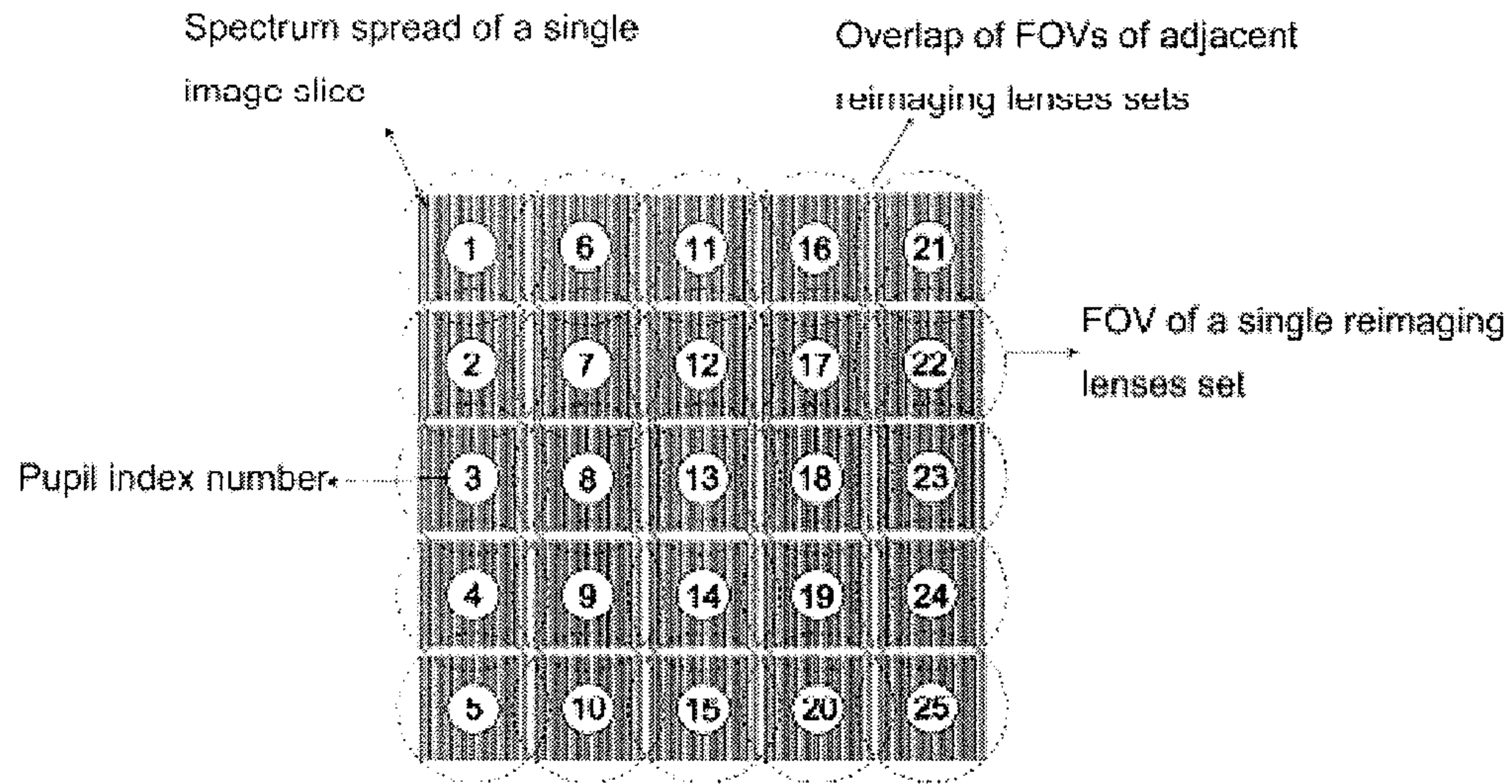
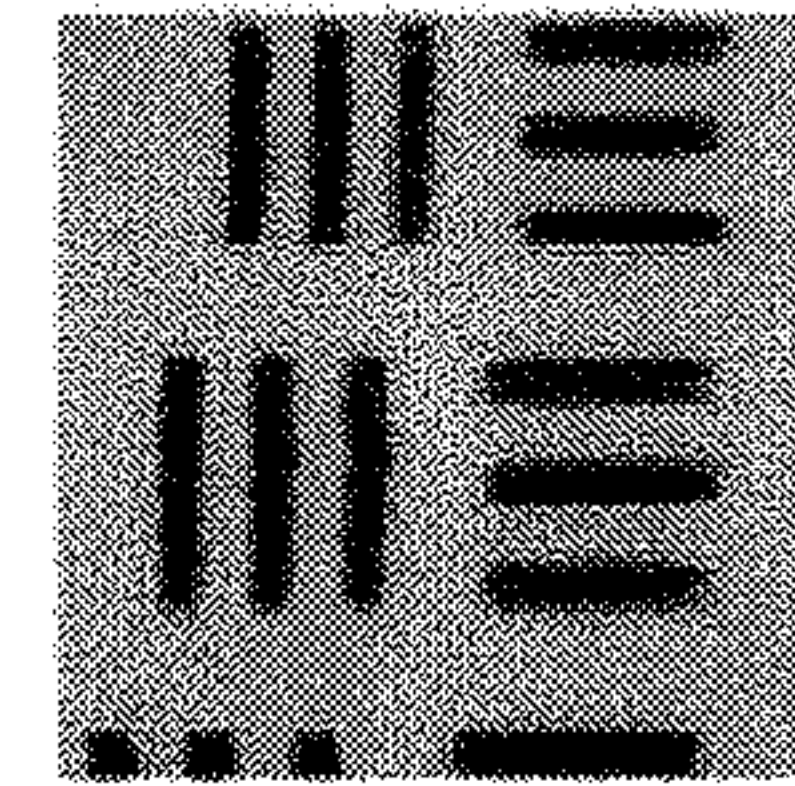
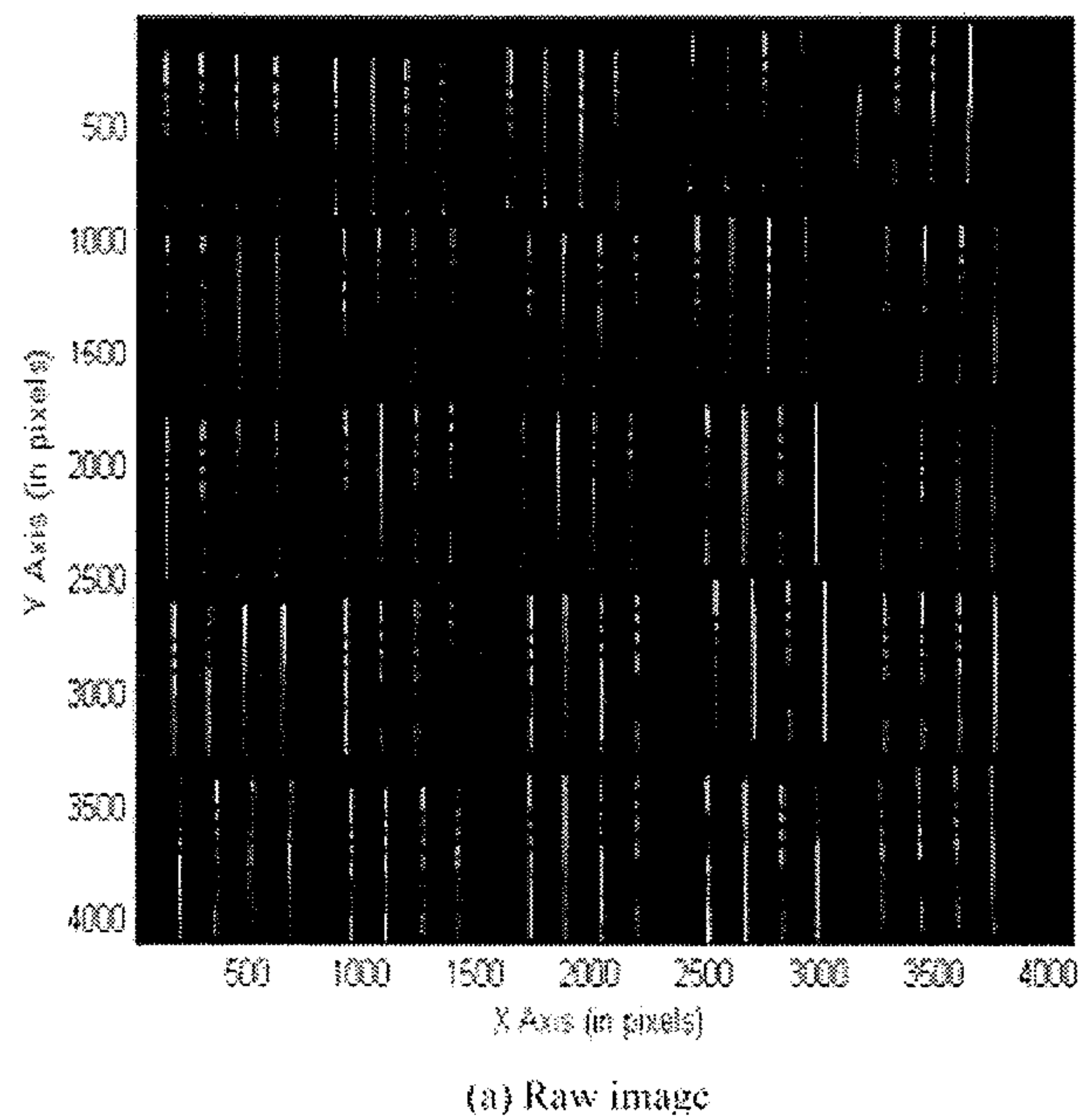
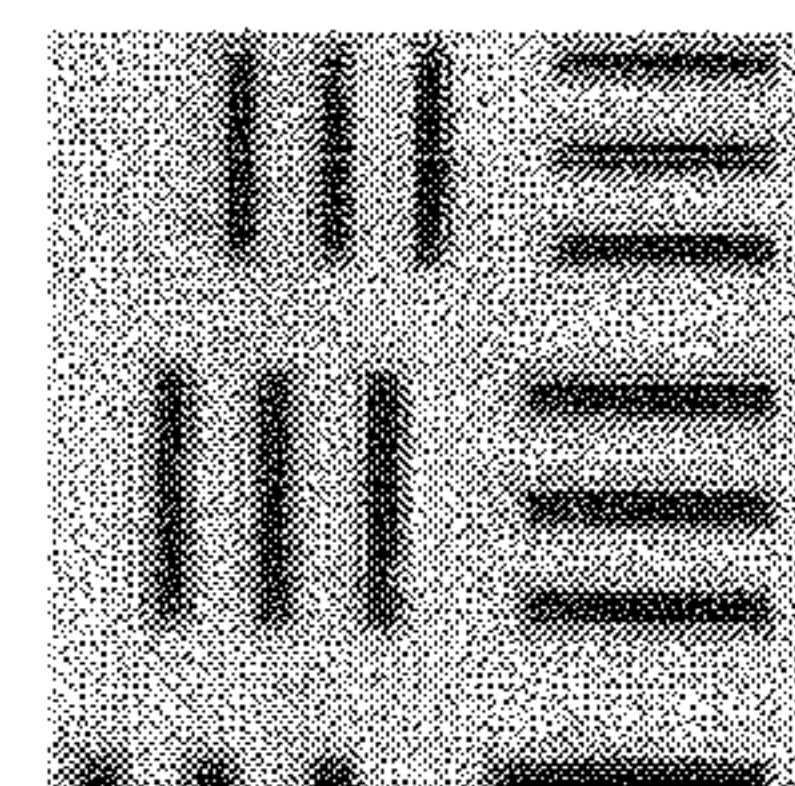


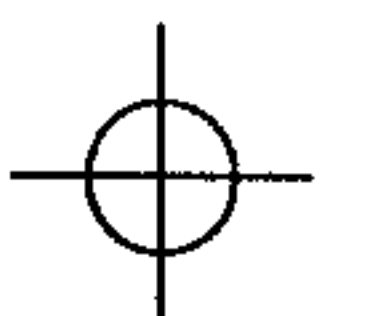
Fig. 33



(b) Reconstructed image



(c) Image directly captured by monochromatic camera



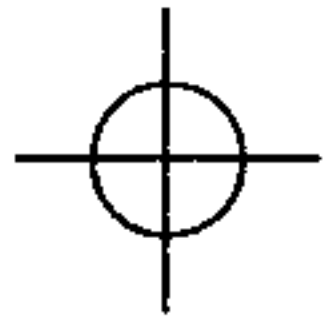
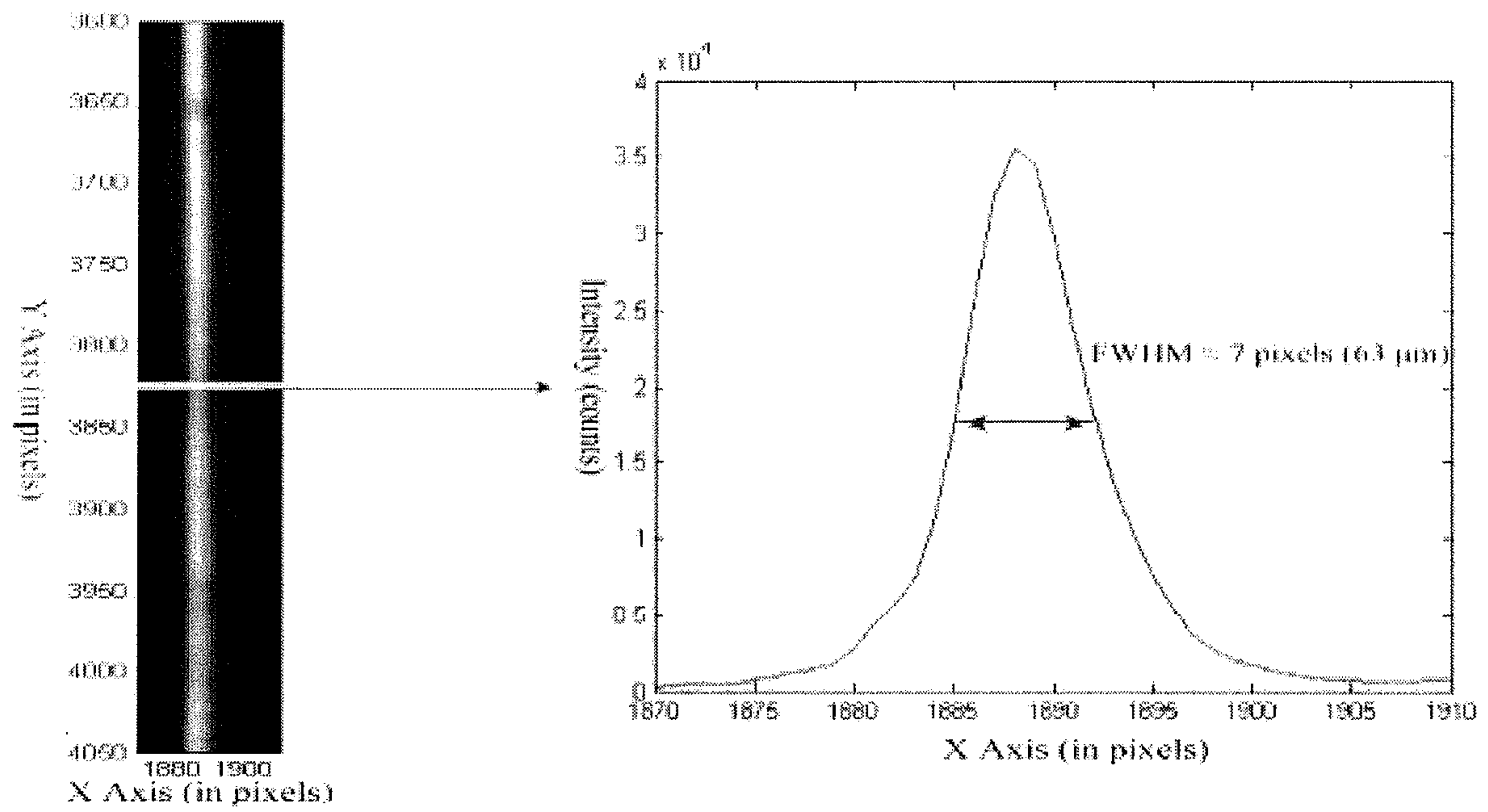
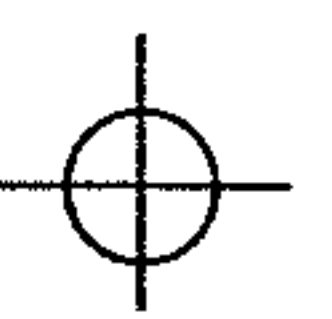


Fig.34



Undispersed slice image

PSF



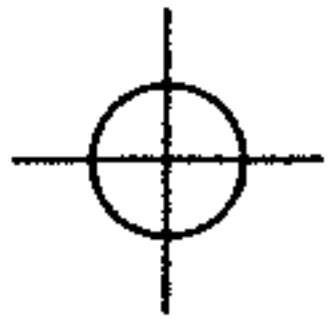
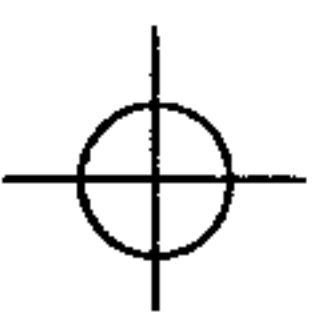
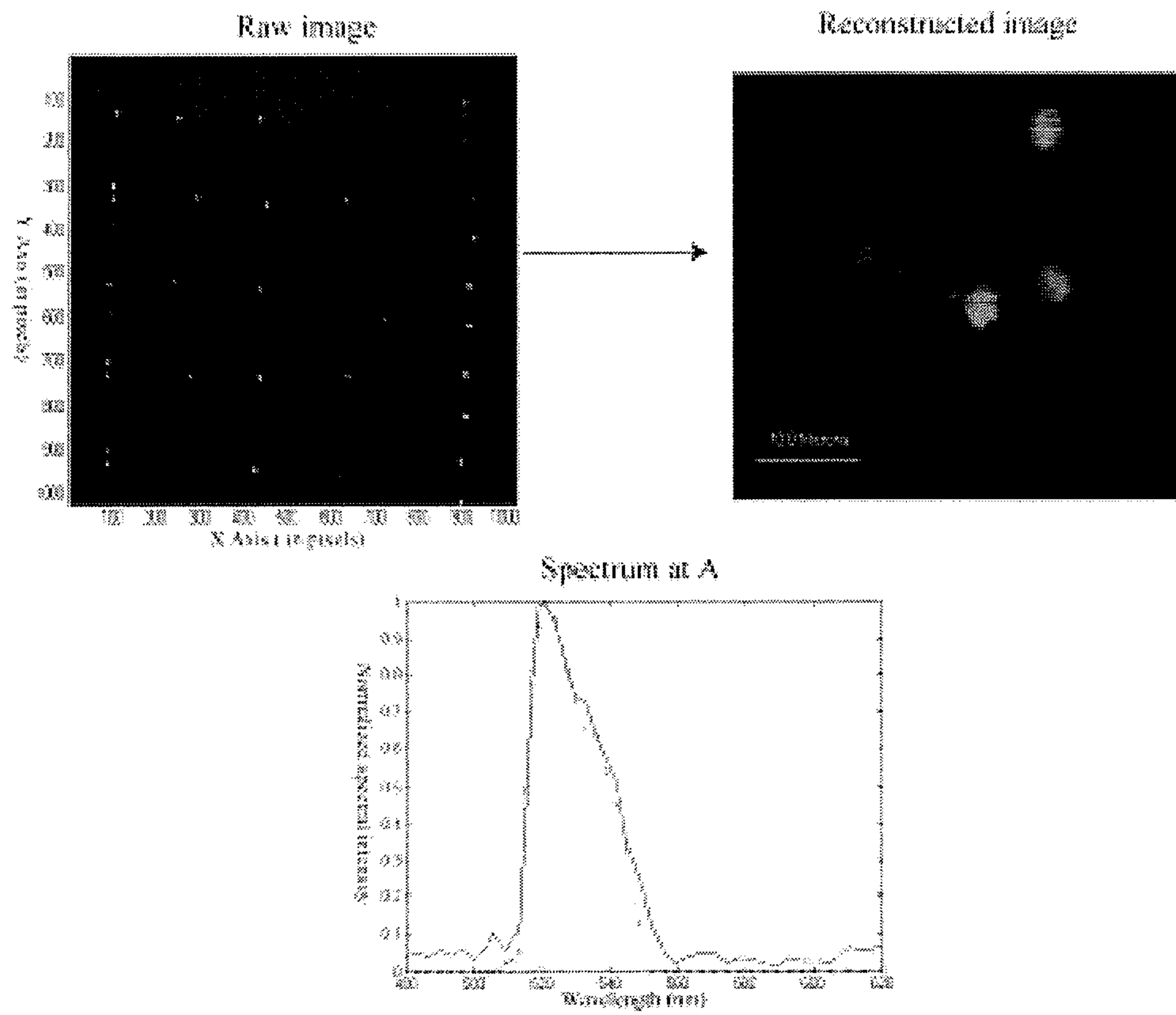


Fig. 35



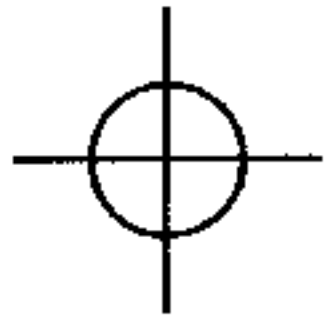
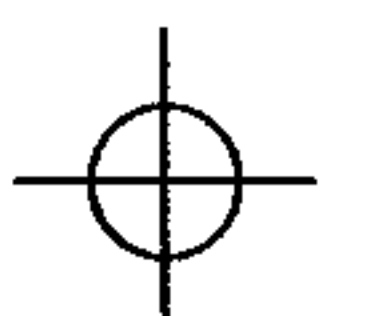
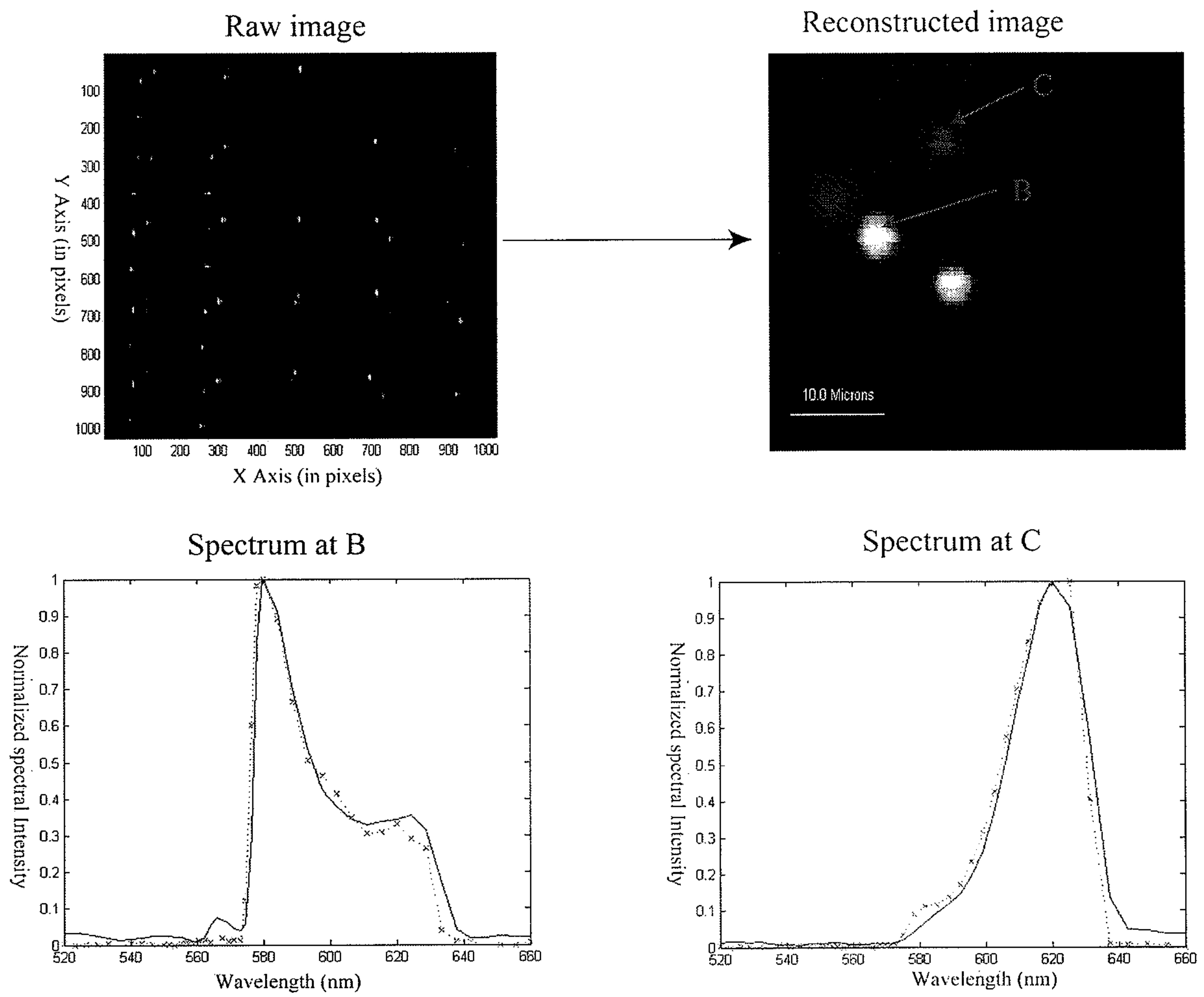


Fig. 36



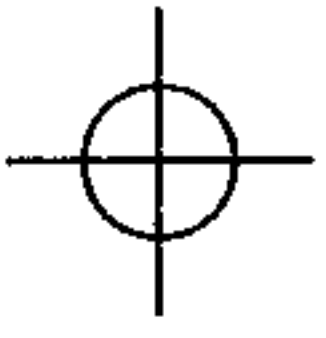
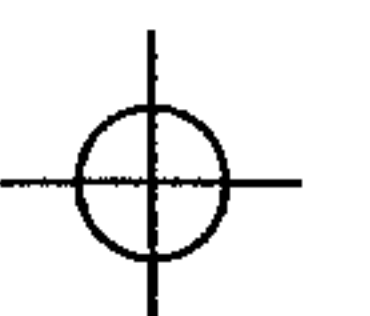
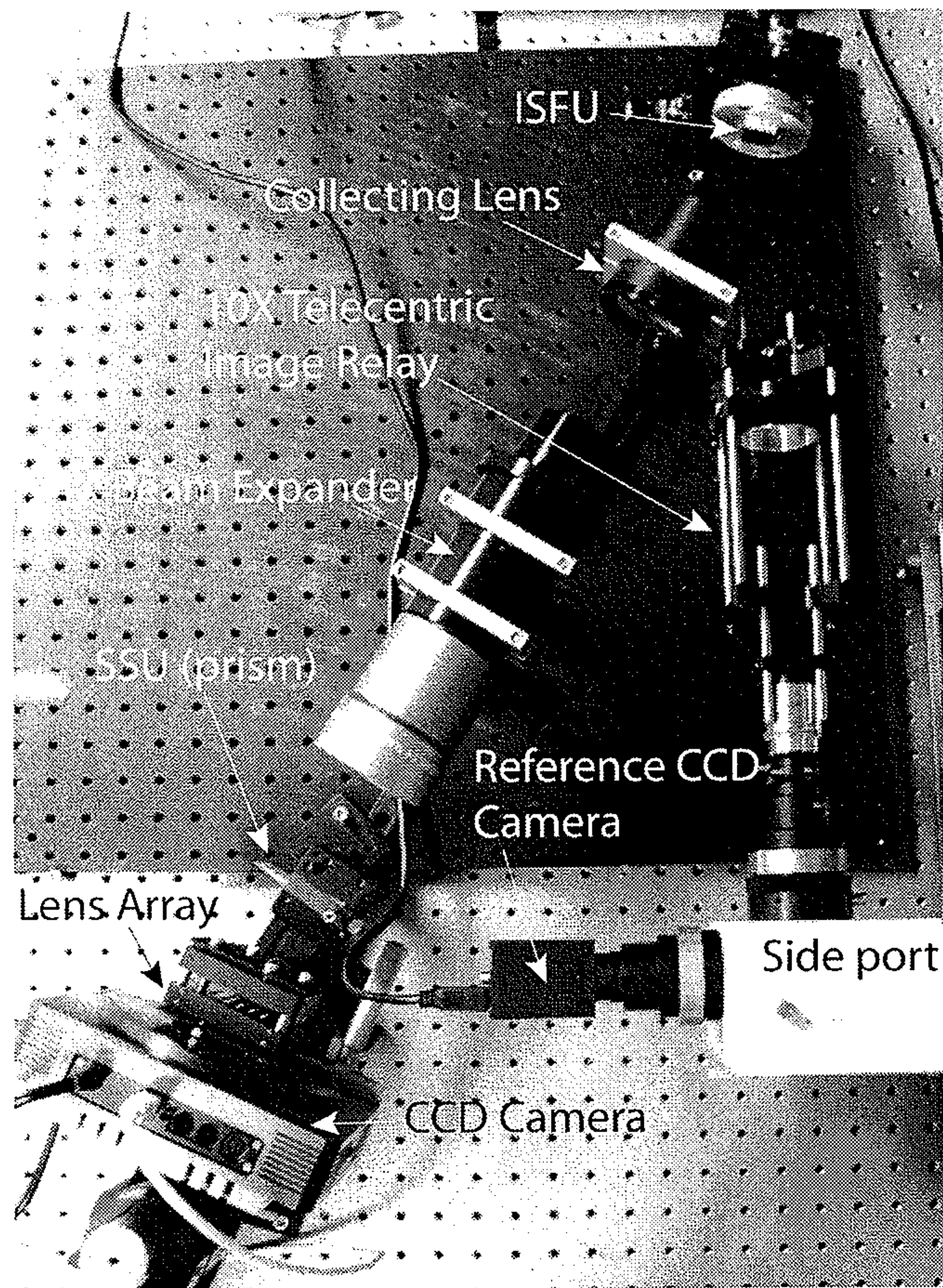


Fig. 37



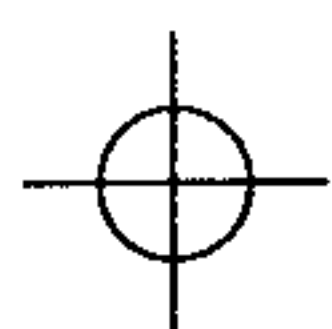
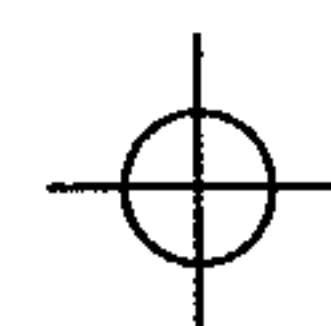
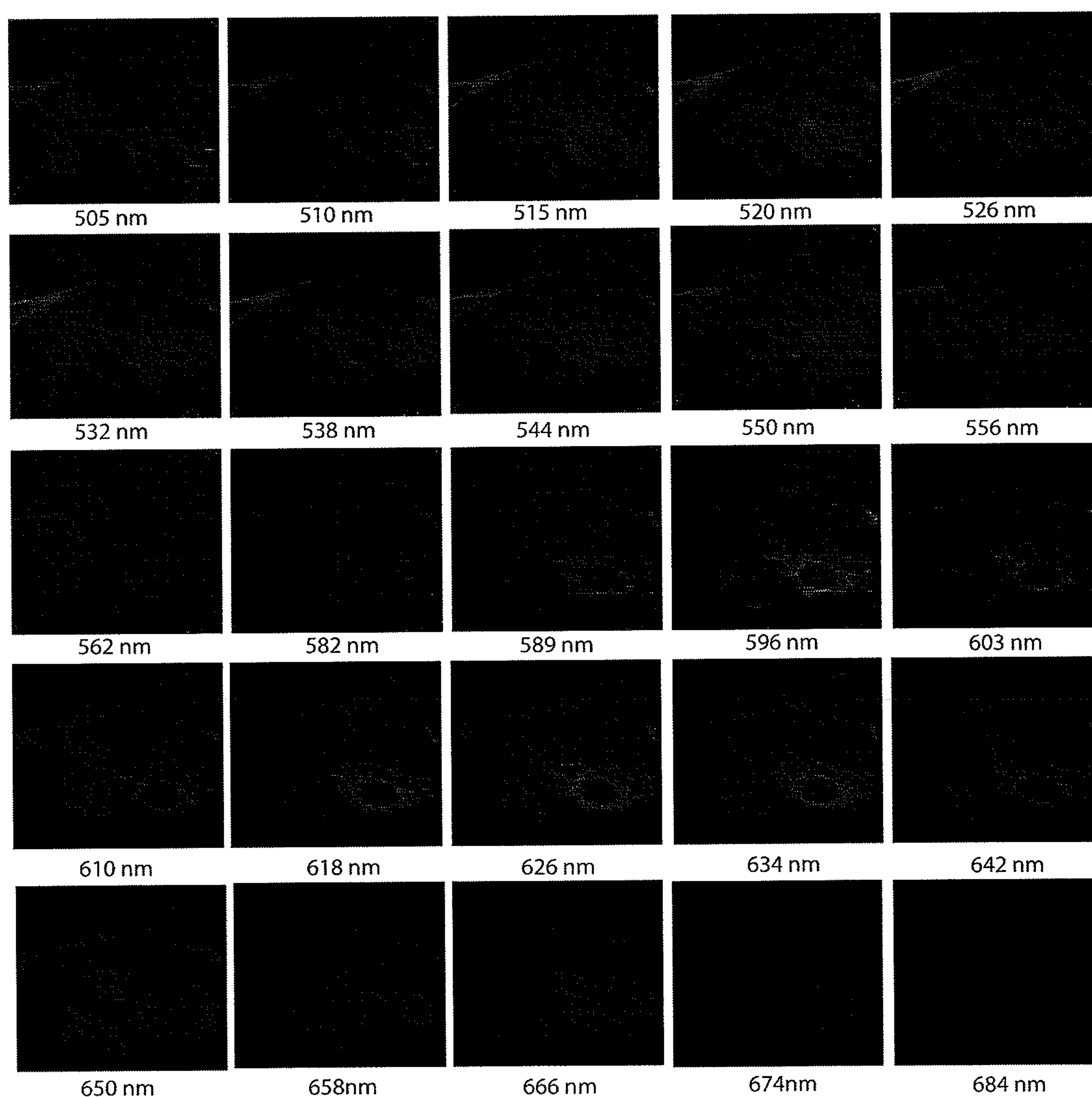


Fig. 38



(Side) Biological sample imaged with reference CCD. Bovine pulmonary artery endothelial cells incubated with MitoTracker Red CMXRos to label the mitochondria. BODIPY FL phalloidin to label the filamentous actin (F-actin) and DAPI to label the nucleus. (Bottom) 25 spectral band images of sample with 5~8 nm spectral spacing from 505-684 nm taken with IMS system.



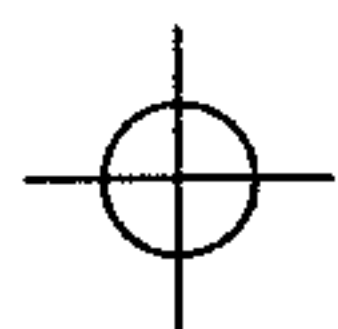
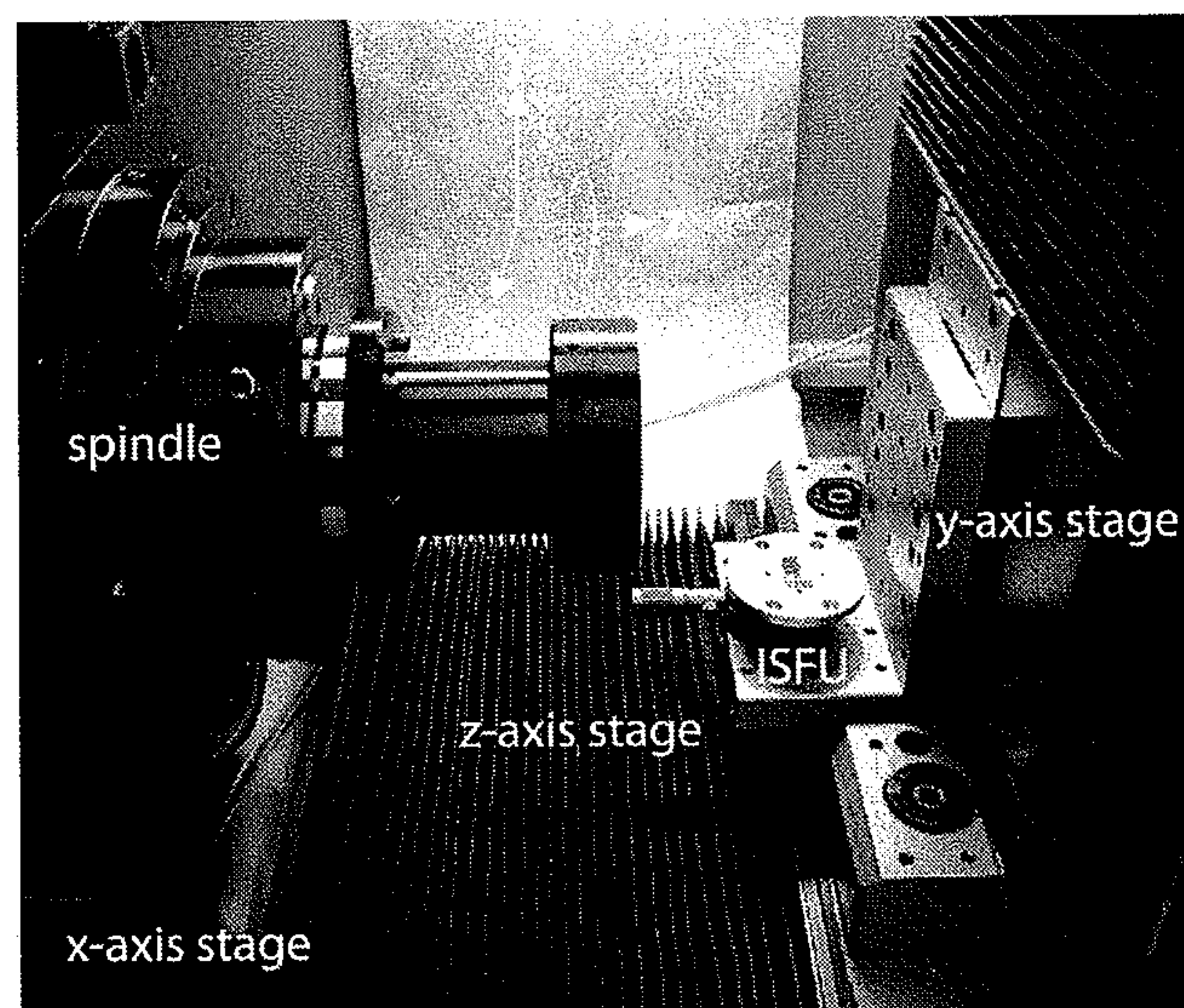
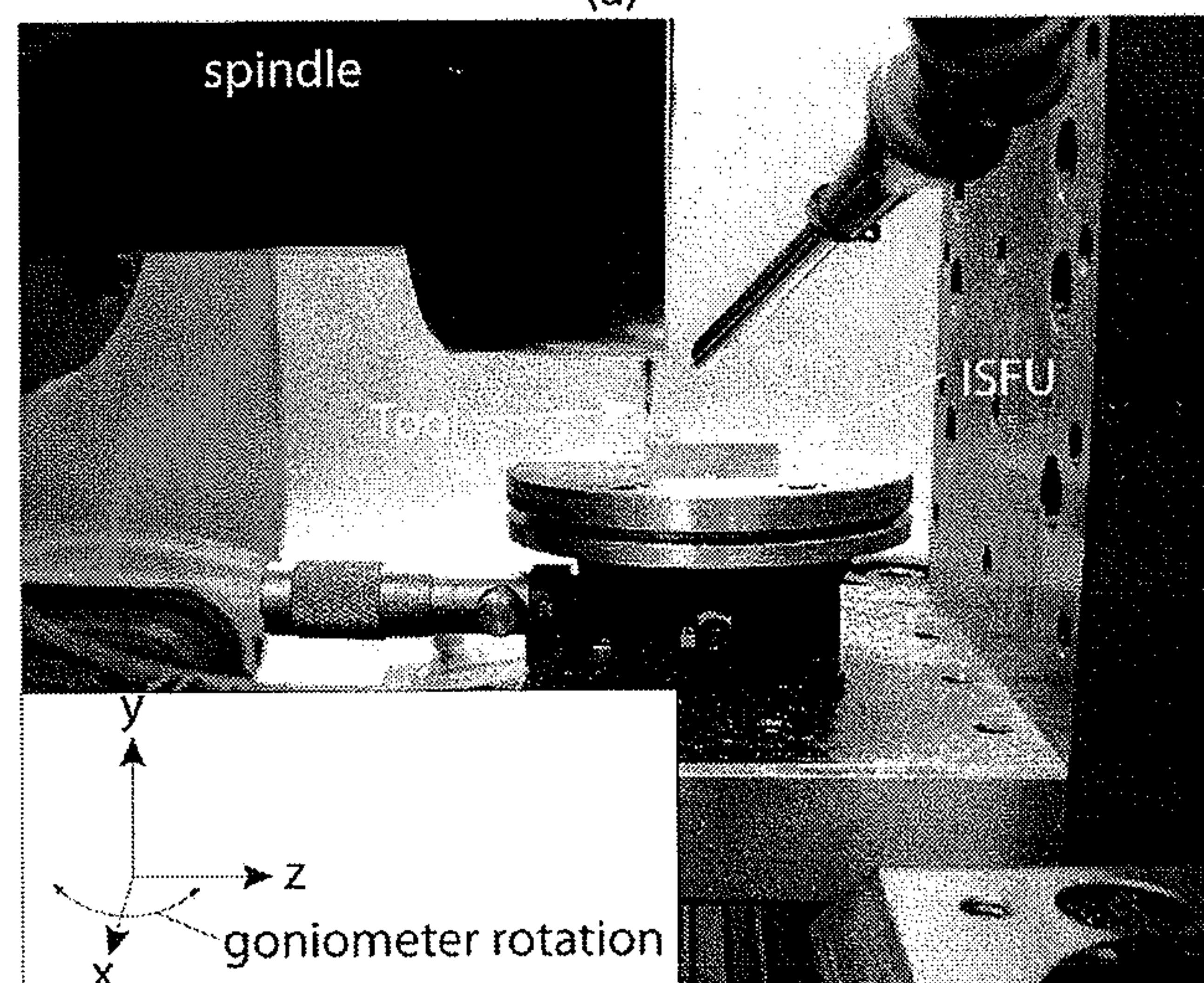


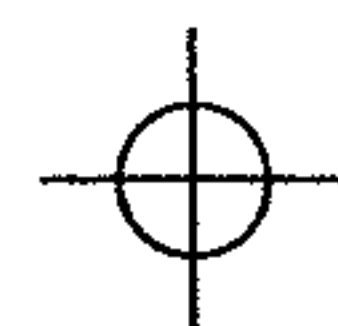
Fig. 39



(a)



(b)



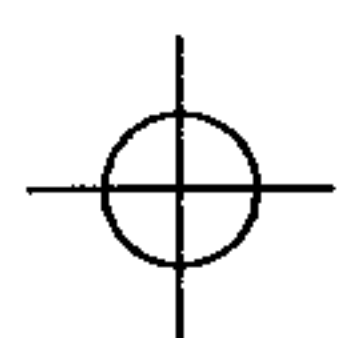
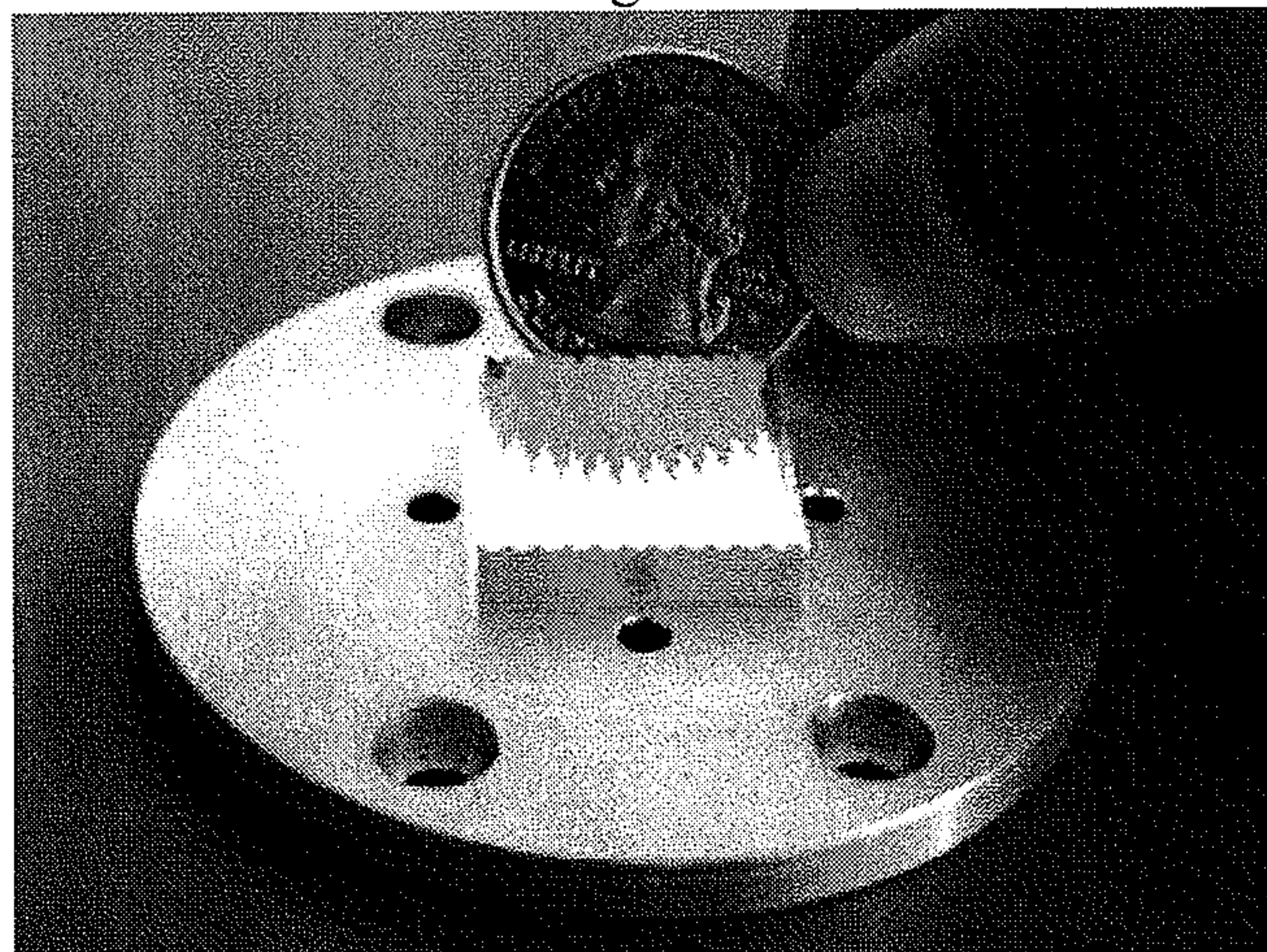
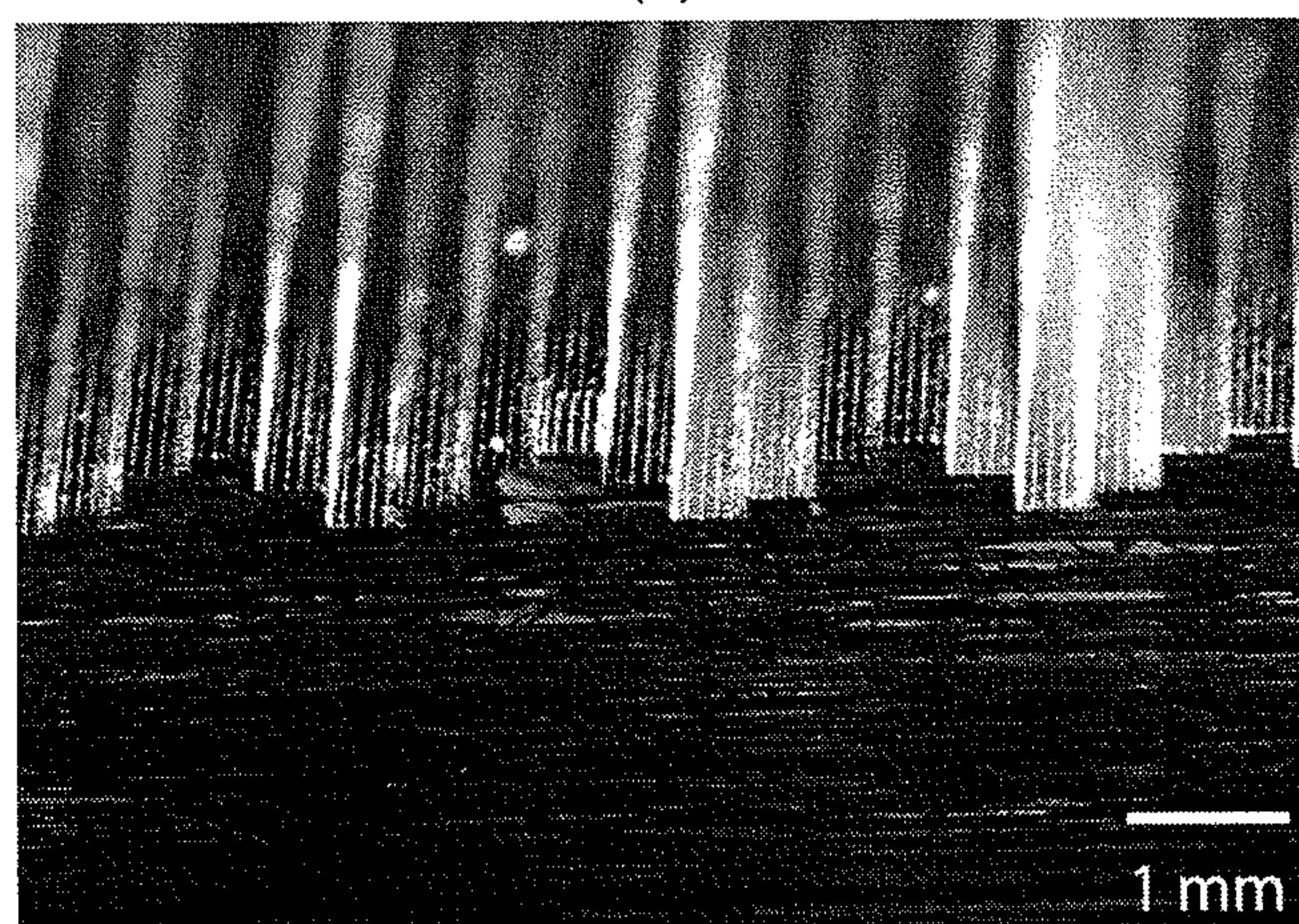


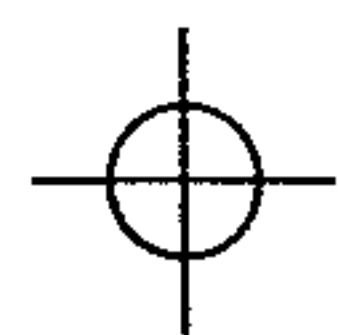
Fig. 40



(a)



(b)



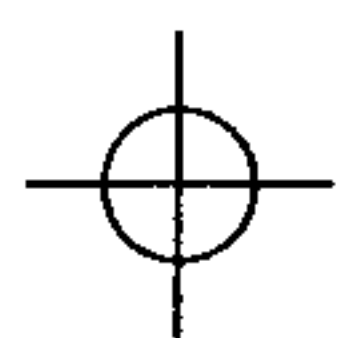


Fig. 41
3D Profile Maps

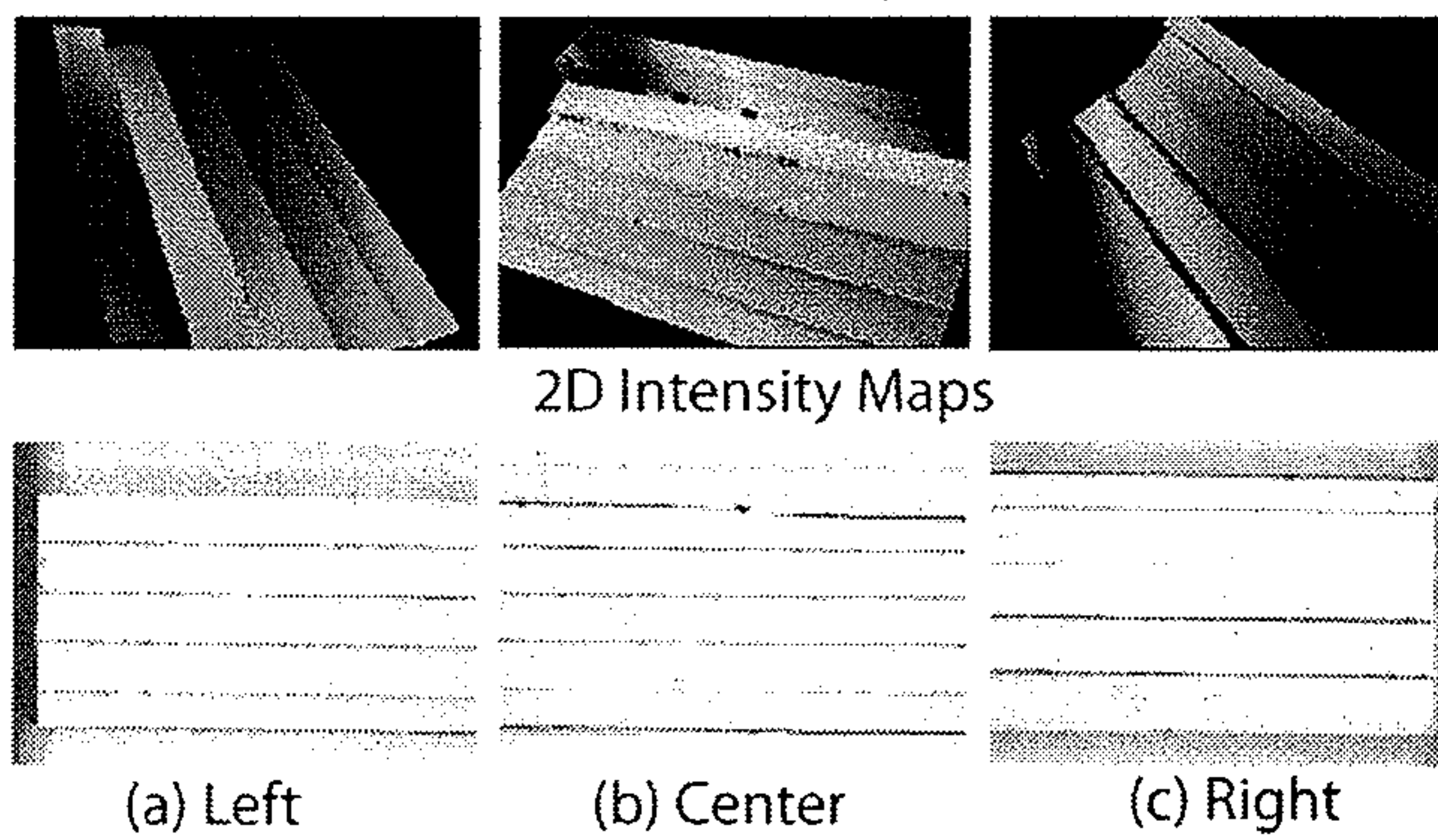


Fig. 42

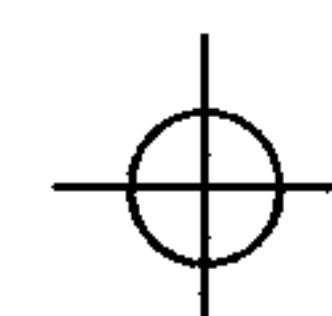
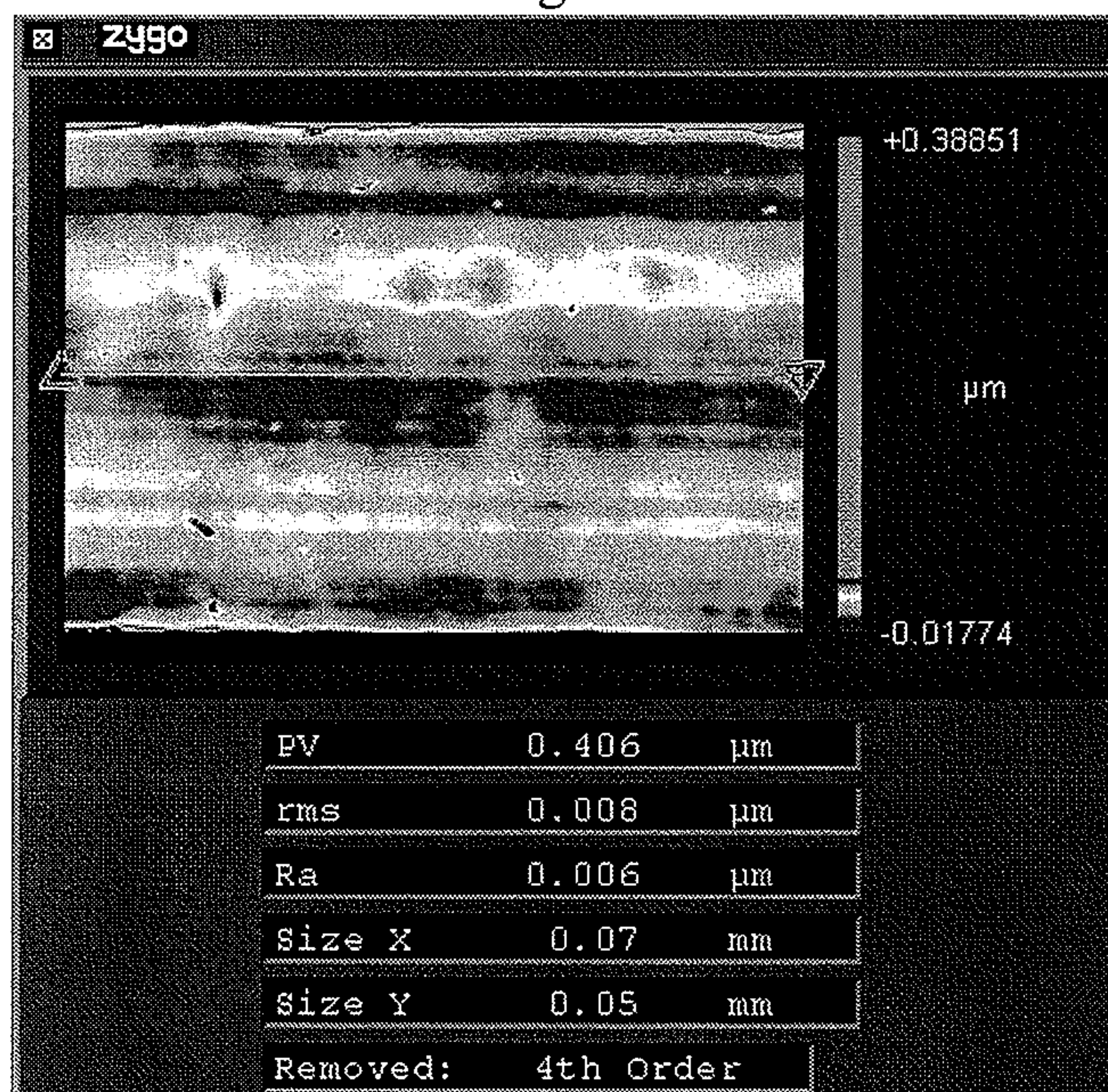


Fig. 2

