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APPLICATION FOR A PATENT OR PATENT OF ADDITION

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of Invention

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Applicants.

(5) Here  
insert (in  
full) Name  
and Address  
of Actual  
Inventor or  
Inventors.

(6) Full Name  
of Actual  
Inventor or  
Inventors.

In support of the Convention Application made by <sup>(1)</sup> BAXTER INTERNATIONAL  
INC., a Corporation of the State of Delaware, United States of America

for a patent ..... for an invention entitled <sup>(2)</sup> CALIBRATING PLURAL PUMP FLUID FLOW SYSTEM

I, <sup>(3)</sup> John F. Gaither, Jr., Assistant Secretary  
of BAXTER INTERNATIONAL INC.,  
Deerfield, Illinois 60015 United States of America

do solemnly and sincerely declare as follows:

1. I am authorised by <sup>(1)</sup> BAXTER INTERNATIONAL INC.,  
the applicant  
for the patent ..... to make this declaration on its behalf.

2. The basic application(s) as defined by Section 141 of the Act was/were made in <sup>(4)</sup> US  
on the 27th day of November 1985, by  
Paul R. Prince

on the ..... day of ..... 1985, by

3. <sup>(5)</sup> Paul R. Prince of 15960 Maidstone Street, Fountain Valley, CA 92708 (US)

is/are the actual inventor(s) of the invention, and the facts upon which <sup>(1)</sup> the applicant company

is entitled to make the application, are as follows:

The said <sup>(1)</sup> BAXTER INTERNATIONAL INC.,  
is the assignee of the said <sup>(6)</sup> Paul R. Prince

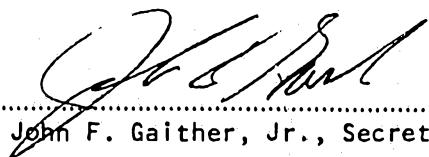
4. The basic application(s) referred to in paragraph 2 of this Declaration was/were the first  
application(s) made in a Convention country in respect of the invention the subject of the  
application.

DECLARED at Deerfield, Illinois 60015 U.S.A.  
22nd day of September 1988

(7) Signature.

To:

THE COMMISSIONER OF PATENTS.

  
(7) John F. Gaither, Jr., Secretary

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(56) Prior Art Documents  
US 4416654  
US 4303193  
US 4197847

(57) Claim

1. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween, said method comprising the steps of:  
automatically controlling said pumps to inject fluid into said common fluid path and/or to withdraw fluid from said common fluid path at respectively associated nominal rates;  
automatically measuring changes in at least one fluid flow parameter occurring within said common fluid path in response to said controlling of said pumps at said respectively associated nominal rates; and  
automatically deriving relative flow calibration data for the individual pumps using said measured changes.

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(10) 597637

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14. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path, said apparatus comprising:

means for controlling said pumps to inject fluid into said path and/or to withdraw fluid from said path at respectively associated nominal rates;

means for measuring changes in at least one fluid flow parameter occurring within said path in response to said injection of fluid into, and withdrawal of fluid from, said common fluid path; and

means for deriving relative flow calibration data for the individual pumps in response to said measured changes.

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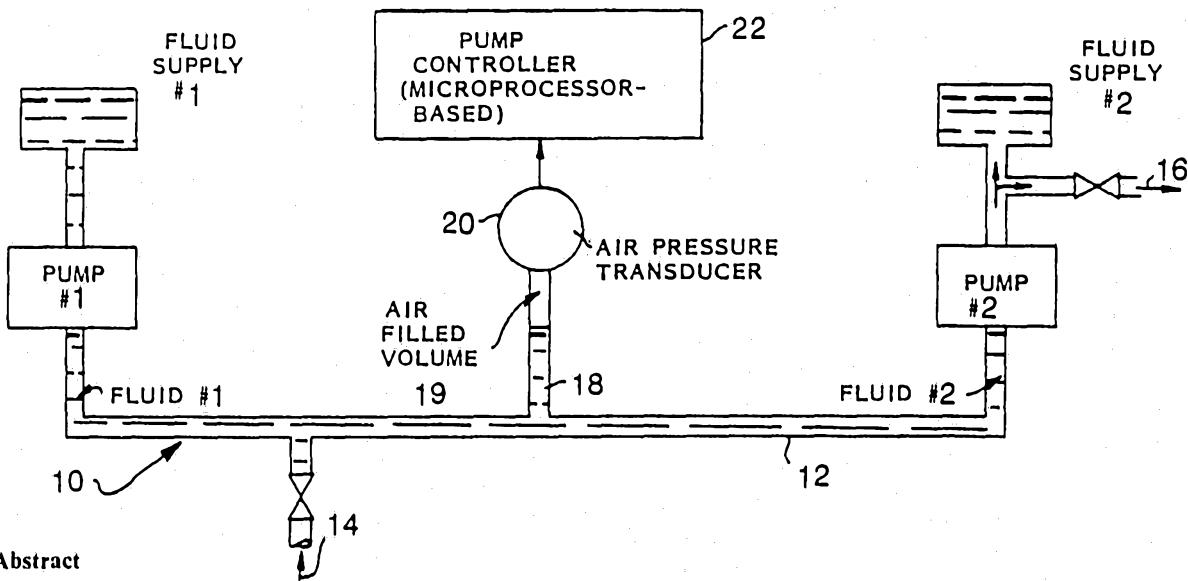
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Section 49 and is correct for  
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(54) Title: CALIBRATING PLURAL PUMP FLUID FLOW SYSTEM



(57) Abstract

A blood constituent processing system (10) uses a disposable plastic fluid flow path (12) into which an anticoagulant must be accurately metered with respect to pumped blood flow. In a preliminary calibration phase, a closed fluid flow path (12) is provided between the anticoagulant pump and the blood pump. One of the pumps is then controlled to inject fluid into such closed path while the other pump is controlled to withdraw fluid from that path at what is nominally an equal fluid flow rate. Changes in fluid pressure within the closed fluid flow path (12) are then monitored (20) and the flow rate of at least one of the pumps is changed as necessary to achieve an approximately constant fluid pressure within the closed fluid flow path (12). The relative pump flow control (22) required to achieve constant pressure may then be taken as a relative flow rate calibration between the two pumps so as to permit subsequent accurate pumped metering of anticoagulant into the pumped blood flow. A similar arrangement may be used to derive relative flow calibration constants for the blood pump and a packed cell pump also present in the blood constituent processing system.

## CALIBRATING PLURAL PUMP FLUID FLOW SYSTEM

This invention generally relates to method and apparatus for calibrating relative pump flow rates between plural pumps in a common fluid flow system. The invention is particularly suited for 5 accurately calibrating relative fluid flow rates achieved by independent pumps within a disposable plastic fluid flow path of a blood constituent processing system.

Where plural independently controlled pumps 10 are included in a common fluid flow system, it is sometimes necessary to accurately calibrate the relative flow rates between the various pumps within the system. For example, a typical blood constituent processing system may add a metered 15 quantity of anticoagulant into a pumped flow of blood constituents. Such requirements may typically arise in a blood plasma filtering system (e.g. where whole blood is extracted from a donor, processed to remove plasma and to return the residual packed red 20 blood cells to the donor) and/or in a platelet separation system (e.g. where whole blood from a donor is processed to remove platelets and/or plasma and the residual blood constituents are returned to the donor).

In such a blood constituent processing 25 system, there may also be a desire to accurately calibrate the relative flow rates of the blood pumped into a filter (or other fractionating device) and the packed cells output from the filter (and/or 30 of the filtrated or separated fraction also being output from the filter).

In such blood constituent processing systems, for obvious health reasons, the fluid flow path is typically defined by disposable plastic

tubing. Such tubing may be manually inserted into conventional pulsatile pumps (e.g. where a rotating member periodically engages and compresses the tubing in a travelling wave type of motion so as to positively displace any fluid contained within the tubing in a pulsatile manner and in a direction determined by the direction of rotation), electromagnetically operated clamps (e.g. to act as "on/off" valves which controllably pinch or close off the plastic tubing at desired control points), etc. The rotational motion of each pump may be electrically monitored using hall-effect pulse generators. In one type of system, a branched section of the tubing includes a trapped 10 compressible gas communicating with a pressure sensor so as to permit fluid pressure variations to be monitored.

Variations from one set of disposable plastic tubing to another (e.g., as further 20 influenced by instantaneous variations in ambient temperature, pressures, flow rates, etc.) may cause significant flow variations. For example, in one exemplary system, the blood pump may experience flow variations of 10% to 15% and the anticoagulant pump 25 may experience variations of up to approximately 10% due to variations from one set of disposable tubing to the next. At the same time, the metering ratio of anticoagulant flow to whole blood flow must typically be controlled with a greater precision to insure proper overall operation of the blood 30 constituent processing system (e.g. for proper platelet survival).

During an initial "priming" mode of such blood constituent processing systems, it is typical to have a fluid flow path (e.g. including the

5 anticoagulant insertion line and the whole blood extraction line) disposed between two pumps (e.g. the anticoagulant metering pump and the whole blood extraction pump) filled with liquid and including an arrangement for monitoring the fluid pressure in this fluid flow path (e.g. a trapped air or other gas or fluid column extending to a pressure sensor).

10 This invention provides method and apparatus for more accurately calibrating the actual fluid flow rates of the anticoagulant pump and the whole blood pump during this initial "set up" or priming mode. For example, the fluid flow path extending between the two pumps may be closed (e.g. 15 by a hemastat or clamp temporarily placed at the juncture of the anticoagulant input tubing and the whole blood extraction tubing) so as to form a closed fluid system between the two pumps (e.g. typically filled with anticoagulant solution and a saline solution and a trapped air or gas region 20 communicating with a pressure sensor). Both pumps may then be commanded to run at the same nominal flow rate and any resulting changes in the monitored pressure of the closed fluid flow system are then 25 detected and used to adjust the commanded pumping rate of at least one of the pumps in a direction and by an amount required to null the value of such detected pressure changes with respect to time.

30 Alternatively, a change with respect to time in the liquid volume within the closed fluid system may be observed and driven to zero. In this configuration, the fluid system between the pumps need not be closed.

At the end of such calibration procedure, one will know the relative pump flow control commands required to actually achieve equal flow

rates and, accordingly, this provides a relative flow rate calibration factor relating the actual flow rate of one pump to the other with a particular set of disposable plastic tubing in place.

5 It is also possible to use this invention to calibrate the blood pump relative to the packed cell pump in a typical plasmapheresis system where the rate of plasma filtrate extraction is determined by the difference between the pumped blood input rate and the pumped packed cell output rate. Here 10 there is also typically an available pressure sensor located in the fluid system between these two pumps. During an initial calibration phase, the plasma filtrate output line may be temporarily 15 clamped shut while the blood pump and packed cell pump rates are adjusted to achieve a constant average fluid pressure therebetween. The required relative pump driving rate then provides a relative fluid flow rate calibration between these two 20 pumps.

Viewed from an overall perspective, the invention thus provides apparatus and method for deriving relative flow characteristics of plural pumps fluid-connected to a common closed fluid path by measuring the relative pump flow controls which 25 are required to maintain an approximately constant average fluid pressure (or a constant average fluid volume) in the path while one pump is injecting fluid and the other pump is withdrawing fluid from the path. Alternatively, it may be possible in some 30 circumstances to measure the time-based rate of pressure change in the fluid path and then to calculate or deduce the required calibration factor based on the measured rate of change. Still further, it may be possible to alternately activate

the individual pumps to inject and/or to withdraw fluid from the closed path while measuring changes in fluid pressure or volume therewithin so as to deduce the relative flow characteristics of the plural pumps connected to the common closed fluid path.

These as well as other objects and advantages of the invention may be better appreciated by carefully studying the following 10 detailed description of a presently preferred exemplary embodiment, when taken in conjunction with the accompanying drawings, of which:

15 FIGURE 1 is a schematic block diagram of an exemplary apparatus which may be used for practicing the method of this invention;

FIGURE 2 is a flow diagram of a suitable computer controlling subroutine or program for the pump controller of FIGURE 1;

20 FIGURE 3 is an explanatory graph depicting typical pressure changes with respect to time in the closed fluid flow path of FIGURE 1;

25 FIGURE 4 is a schematic depiction of a portion of a blood constituent processing system which embodies a closed fluid flow path between two independently controlled pumps in a manner which is similar to that depicted in FIGURE 1;

FIGURE 5 is a schematic block diagram of a control system which may be suitable for

use as the controller in the apparatus of FIGURES 1 and/or 4;

5 FIGURE 6 is similar to FIGURE 4 but depicts a different portion of a blood constituent processing system where a blood pump and a packed cell pump are flow calibrated relative to one another; and

10 FIGURE 7 is a graphical depiction of pressure changes versus pump flow error rate.

The system of FIGURE 1 includes plural pumps (e.g. pump #1 and pump #2) interconnected by a closed fluid flow path 12 (e.g. a disposable plastic tubing as in a blood constituent processing system).  
15 In the exemplary embodiment, pump #1 and pump #2 are both peristaltic pumps of conventional design. During sustained system operation, a fluid may be input at 14 (e.g. whole blood) and mixed with a metered supply of fluid #1 (e.g. an anticoagulant solution) while being pumped onward to other portions of the apparatus at 16 (e.g. to a plasma or platelet separator/filter device, etc.). Another fluid supply #2 may also be connected with pump #2 (e.g. so as to provide a source of saline solution  
20 during initial priming mode operations or the like). A pressure measuring branch 18 of the closed fluid flow path may typically include a trapped air portion communicating with an air pressure transducer 20. An overall system controller may include a microprocessor-based pump controller 22 which is capable of independently controlling the flow rates of pump #1 and pump #2 and which also has  
25  
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access to pressure data derived from the air pressure transducer 20. Those in the art will recognize that there may be many other configurations of a closed fluid flow path extending between plural pumps which may be independently controlled and for which accurate relative flow rate calibration factors are desired.

In this exemplary embodiment, the relative pump flow calibration system includes a closed fluid flow path which has both incompressible liquids and compressible gases therewithin such that that gas pressure can be used to monitor pressure variations. A relative flow rate calibration of the two pumps with respect to each other is obtained by constraining the system to pump into the closed flow path with one pump and to pump out of the closed flow path with the other pump using nominally identical flow commands. If the pumps actually have equal flow rate calibration factors, then there should be a substantially constant pressure maintained within the interconnecting closed fluid flow path. By monitoring any detected pressure (or contained fluid quantity) variations within the closed fluid flow path, any calibration errors can be detected.

The hardware architecture of the microprocessor-based pump controller 22 may be of conventional design (e.g. a microprocessor chip, RAM/ROM chips, I/O chips, analog-to-digital converters, etc. conventionally interconnected). Similarly, insofar as an understanding and utilization of the present invention is concerned, the computer controlling program or software during normal system operation may be of conventional design (possibly modified so as to include a

multiplicative calibration factor when generating pump control commands).

However, during a calibration period, the controller 22 also may be programmed so as to practice the method of this invention. One example of such a program is depicted in the flow chart of FIGURE 2 (albeit those in the art will recognize that, in accordance with the principles of this invention as here explained, one may devise many different but suitable computer programs). A "hardwired" controller can also be readily designed to practice this invention as will also be readily appreciated by those in the art.

Upon entry into the pump calibrate subroutine 200 of FIGURE 2, some initial "housekeeping" details may be attended to such as those depicted at block 202. For example, a counter N may be reset to a contents of 1 and a visual operator display may be activated so as to request closure of the fluid path interconnecting the plural pumps in the system (e.g. by closing the valves near inlet 14 and outlet 16 or by applying suitable hemostats, clamps, etc.) Alternatively, if the system includes suitably placed electromagnetically controlled tubing clamps or the like, then the controller 22 may automatically close off a fluid flow path interconnecting the plural pumps in the system.

A check may be made at step 204 for the existence of a closed fluid system (e.g. by monitoring a manually activated switch and/or by performing automated stimulus/response testing routines as will be apparent). Once a properly closed fluid system is in place, control is passed to step 206 where pump #1 is activated to insert

fluid into the closed system at a pump rate X while pump #2 is simultaneously activated to extract fluid from the closed system at pump rate Y -- the nominal pump rates X and Y being initially selected to be 5 equal.

A pressure reading is then taken at 208 (possibly after some finite "settling" time to permit start up of the pumps) after which a wait loop is entered at step 210 (e.g. 4.25 seconds).

10 Upon exit from the wait loop 210, a new pressure reading is taken at 212 and tested at 214 so as to detect any pressure changes in excess of some predetermined positive or negative "noise" value. If a significant pressure change is detected, then 15 in block 215 a correction term proportional to the error (through multiplication factor Kg) is applied, and control is passed to block 216 where it is determined whether the pressure change is in the increasing or decreasing direction. If the pressure 20 change increased, then the pump rate Y of pump #2 is increased (or, alternatively, the pump rate X is decreased) by the correction term and control is passed back to the wait loop 210. On the other hand, if the pressure change was in the decreasing 25 direction, then pump rate Y is decreased (or, alternatively, pump rate X is increased) by a suitable correction term and control is again passed back to the wait loop 210.

If no significant pressure change is 30 observed, then the N counter is tested at 222 to see if it yet equals a maximum preset value corresponding to the required time interval of approximately constant pressure. If the required constant pressure period is not yet at hand, then the N counter is incremented at 224 and control is

passed back to the wait loop 210. On the other hand, after a sufficiently long period of constant pressure has been detected, then exit will be made to block 226 where the then existing relative pump rates X, Y will be stored away as pump flow calibration factors and a normal exit may be made at 228 from the pump calibrate subroutine.

A typical graph of pressure variations within the closed flow path as a function of time during operation of the calibration process is depicted at FIGURE 3. Here, it will be seen that an initial portion of the pressure versus time curve exhibits a slope which itself indicates the relative pump calibration error. As will be understood, it may be possible to measure the value of this slope and calculate the appropriate pump flow calibration factors X, Y directly based upon such a slope measurement. However, such measurement involves some error since slope is proportional to flow rate errors and volume of trapped air 19 (see FIGURE 1). After matched pump calibration has been achieved, it will be seen in FIGURE 3 that the slope of the pressure versus time curve reduces to an approximately zero value.

FIGURE 4 is similar to FIGURE 1 but more realistically depicts a portion of a typical blood constituent processing system and a portion of a typical disposable plastic tubing harness which is typically threaded into various pumping, clamping, pressure sensing, etc. apparatus which is, in turn, under control of a microprocessor-based controller. During a priming mode, the fluid flow path between the anticoagulant pump and the blood pump is filled with liquid (thereby trapping a quantity of air in a pressure measuring branch of the tubing

communicating with the pressure sensor). A hemostat or clamp is then placed at the junction of the anticoagulant tubing and of the blood extraction tubing so that the two liquids (anticoagulant solution and saline solution in this preliminary priming mode) form a closed system between the two pumps, with the air region and pressure sensor monitoring the closed system.

Pressure then builds up or falls as the two pumps are commanded to produce the same nominal flow rate. A control system such as that depicted in FIGURE 5 automatically observes the pressure changes over a time period and responsively controls at least one of the pumps to change its actual flow rate. As previously mentioned, the necessary calibration factor relating the relative actual flow rates of the pumps with a given disposable plastic tubing harness in place may be obtained by measuring the slope or rate of change of the pressure versus time curve and/or by empirically modifying the relative pump calibration factors so as to null any detected pressure changes. For example, a modified pump flow constant may be generated so as to direct one of the pumps actually to rotate faster or slower for a specified nominal liquid flow rate. After sufficient precision has been attained, the calibration procedure is complete.

In one exemplary embodiment, as depicted in FIGURE 5, both pumps are initially commanded to flow at a rate of 10 milliliters per minute as represented schematically at block 500 in FIGURE 5. This command is multiplied by an anticoagulant pump flow constant or calibration factor X at block 502 and by a blood pump flow constant or calibration factor Y at block 504 before actually being used to

control the speed of the anticoagulant pump at block 506 and the blood pump at 508. The two pumps then act upon the closed fluid vessel system (including air) as depicted at block 510 and cause an air pressure response which is measured at block 512. A timed sampler 514 then feeds a gain adjustment control block 516 where the calibration factors X, Y are adjusted relative to one another so as to correct for any noted pump flow rate errors.

Another portion of a typical blood constituent processing system is depicted in FIGURE 6. Here the disposable plastic tubing extends on the output side of the blood pump to a plasma filter and on to a pumped packed cell output flow from the filter. In operation, the flow rate of plasma filtrate (e.g., 6 ml/min) may be determined by controlling the pumped rate of blood input (e.g., 50 ml/min) relative to the pumped rate of packed cell output (e.g., 44 ml/min). As in the FIGURE 4 embodiment, a branch of tubing between the two pumps includes a volume of trapped air communicating with a pressure transducer. After the system is filled with liquid, the blood pump may be operated near the expected rate of use (or perhaps initially slower) while the plasma filtrate output is clamped shut and the packed cell pump is operated at a nominally equal rate. The pressure P2 will begin to rise or fall due to any difference in actual pump rates. That compliance due to the air pocket in the tubing to the pressure transducer keeps the pressures within reasonable bounds for initial errors in flow rates. Typically, this calibration procedure may be performed after some initial filtration has occurred and blood plasma has already filled the plasma

filter and tubing down to the clamp point on the plasma output tube.

5 FIGURE 7 illustrates the resulting pressure profile and its first derivative (with respect to time) for a regularly changing relative difference in pump flow rates. An iterative or other procedure may then be employed (as before) to determine relative pump flow rate calibration factors which may thereafter be used to achieve accurate relative 10 pump flow rates. Following such measurement, the relative flow rates can be temporarily shifted to bring the pressure within a normal range (e.g., as measured just prior to plasma clamp closure) before re-opening the plasma clamp.

15 As will now be appreciated, if one of the pumps can also be calibrated with respect to an absolute standard (e.g., if the packed cell pump delivers its output to a collection reservoir which is carried by an electronic weighing or other 20 volume/mass/weight measuring device), then one can, in turn, use the relative pump flow calibration factors to derive absolute calibration factors for the other pump(s).

25 If pulsatile pumps are employed, there will, of course, be periodic pressure/volume pulses which may be disregarded (e.g., by employing suitable low pass "averaging" filters) in the calibration procedures.

30 While only a few exemplary embodiments have been explained in detail, those skilled in the art will recognize that many modifications and variations may be made in these exemplary embodiments while yet maintaining many of the novel features and advantages of this invention. Accordingly, all such modifications and variations

are to be included within the scope of the appended claims.

THE CLAIMS DEFINING THE INVENTION ARE AS FOLLOWS:

1. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween, said method comprising the steps of:

automatically controlling said pumps to inject fluid into said common fluid path and/or to withdraw fluid from said common fluid path at respectively associated nominal rates;

automatically measuring changes in at least one fluid flow parameter occurring within said common fluid path in response to said controlling of said pumps at said respectively associated nominal rates; and

automatically deriving relative flow calibration data for the individual pumps using said measured changes.

2. A method as in claim 1 wherein said controlling step comprises controlling a first pump to inject fluid into said path at a first nominal rate and controlling a second pump to withdraw fluid from said path at a second nominal rate, at least one of said rates being controlled to maintain an approximately constant fluid pressure in said path.

3. A method as in claim 1 wherein said controlling step comprises controlling a first pump to inject fluid into said path at a first nominal rate and controlling a second pump to withdraw fluid from said path at a second nominal rate, at least one of said rates being controlled to maintain an approximately constant fluid volume in said path.



4. A method as in claim 1 wherein:

said controlling step comprises controlling a first pump to inject fluid into said path at a first nominal rate and controlling a second pump to



withdraw fluid from said path at a second nominal rate; and

said measuring step comprises measuring the rate-of-change in fluid pressure in said path.

5. A method for deriving relative flow characteristics of plural pumps connected with a common fluid path, said method comprising the step of:

measuring the relative pump flow controls which are required to maintain an approximately constant fluid pressure in said path while one pump is injecting fluid into said path and another pump is withdrawing fluid from said path.

6. A method for deriving relative flow characteristics of plural pumps connected with a common fluid path, said method comprising the step of:

measuring the relative pump flow controls which are required to maintain an approximately constant fluid volume in said path while one pump is injecting fluid into said path and another pump is withdrawing fluid from said path.

7. A method for deriving relative flow characteristics of an anticoagulant pump and a blood pump connected in a blood constituent processing system with a disposable plastic tubing which includes a common fluid path, said method comprising the steps of:

installing a disposable plastic tubing into a blood constituent processing system and providing a common closed fluid path within the disposable

tubing and extending between an anticoagulant pump and a blood pump;

controlling the pumps to inject and/or withdraw fluid from said path at respective nominal rates;

measuring a predetermined fluid parameter in said path during said controlling step; and

deriving said relative flow characteristics in response to the controlling and/or measuring steps.

8. A method as in claim 7 wherein said controlling step comprises simultaneously

(a) controlling a first pump to inject fluid into said path at a first nominal rate, (b) controlling a second pump to withdraw fluid from said path at a second nominal rate, and (c) changing at least one of said controlled nominal rates so as to maintain an approximately constant measured fluid pressure or volume in said path.

9. A method as in claim 8 wherein said deriving step comprises recording the relationship between the nominal pump flow rates required to maintain said approximately constant fluid pressure.

10. A method as in claim 7 wherein said deriving step comprises measuring the time-based rate of pressure change in said path.

11. A method for obtaining a relative flow calibration factor for a system of plural pumps connected with a common fluid flow path, said method comprising:

controlling at least two of the pumps to simultaneously inject and withdraw fluid from said path at relative rates which approximately maintain a constant fluid pressure or volume within said path; and

measuring at least one relative pump flow calibration factor for said at least two pumps based on the controlled pumping rates required to approximately maintain said constant fluid pressure or volume.

12. A method for calibrating relative pump flow rates of plural pumps connected with a common fluid-containing structure, said method comprising:

controlling at least one of said pumps to pump liquid into said structure at a first nominal rate;

simultaneously controlling at least one other of said pumps to pump liquid out of said structure at a second nominal rate;

monitoring the fluid pressure or volume within said structure during said controlling step; and

adjusting at least one of said nominal pump rates in response to said monitored fluid pressure or volume so as to obtain calibrated relative pump flow rates between plural pumps.

13. A method for calibrating a first pump flow with respect to a second pump flow in a blood constituent processing system, said method comprising the steps of:

installing a disposable plastic tubing into said blood constituent processing system which

includes a common fluid flow path between said first pump and said second pump;

pumping fluid into said path with one of said pumps at a first predetermined nominal rate and pumping fluid out of said path with the other of said pumps at a second predetermined nominal rate, which rates are initially set to be at assumed equal values;

detecting changes in fluid pressure or volume within said path caused by said pumping step;

adjusting at least one of said first and second rates in response to said detecting step so as to maintain an approximately constant fluid pressure or volume within said path; and

deriving a relative pump flow calibration factor based on the controlled nominal flow rates required by said adjusting step.

14. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path, said apparatus comprising:

means for controlling said pumps to inject fluid into said path and/or to withdraw fluid from said path at respectively associated nominal rates;

means for measuring changes in at least one fluid flow parameter occurring within said path in response to said injection of fluid into, and withdrawal of fluid from, said common fluid path; and



means for deriving relative flow calibration data for the individual pumps in response to said measured changes.

15. Apparatus as in claim 14 wherein said means for controlling controls a first pump to inject fluid into said path at a first nominal rate and controls a second pump to withdraw fluid from said path at a second nominal rate which is



controlled to maintain an approximately constant fluid pressure or volume in said path.

16. Apparatus as in claim 14 wherein:  
said means for controlling controls a first pump to inject fluid into said path at a first nominal rate and controls a second pump to withdraw fluid from said path at a second nominal rate; and  
said means for measuring measures the rate-of-change in fluid pressure or volume in said path.

17. Apparatus for deriving relative flow <sup>calibration data</sup> characteristics of plural pumps connected with a common closed fluid path, said apparatus comprising:  
means for independently controlling plural pumps connected with a common closed flow path; and  
means for measuring the relative pump flow controls which are required to maintain an approximately constant fluid pressure or volume in said path while one pump is injecting fluid into said path and another pump is withdrawing fluid from said path.

18. Apparatus for deriving relative flow <sup>calibration data</sup> characteristics of first and second pumps connected in a blood constituent processing system with a disposable plastic tubing which includes a common fluid path between said pumps, said apparatus comprising:

a disposable plastic tubing disposed in a blood constituent processing system and providing a common closed fluid path within the disposable tubing and extending between said first pump and said second pump;



means for controlling the pumps to inject and/or withdraw fluid from said path at respective nominal rates;

means for measuring a predetermined fluid parameter in said path; and

means for deriving said relative flow <sup>calibration data</sup> characteristics in response to the effected pump control and/or the measured parameter.

19. Apparatus as in claim 18 wherein said means for controlling simultaneously (a) controls a first pump to inject fluid into said path at a first nominal rate, (b) controls a second pump to withdraw fluid from said path at a second nominal rate, and (c) changes at least one of said controlled nominal rates in response to said means for measuring so as to maintain an approximately constant measured fluid pressure in said path.

20. Apparatus as in claim 19 wherein said means for deriving records the relationship between the nominal pump flow rates required to maintain said approximately constant fluid pressure.

21. Apparatus as in claim 18 wherein said means for deriving measures the time-based rate of pressure change in said path.

22. Apparatus comprising:

a system of plural pumps connected with a common fluid flow path;

means for controlling at least two of the pumps to simultaneously inject and withdraw fluid from said path at relative rates which approximately



maintain a constant fluid pressure or volume within said path; and

means for measuring at least one relative pump flow calibration factor for said at least two pumps based on the controlled pumping rates required to approximately maintain said constant fluid pressure or volume.

23. Apparatus comprising:

plural pumps connected with a common fluid-containing volume;

means for controlling at least one of said pumps to pump liquid into said volume at a first nominal rate;

means for simultaneously controlling at least one other of said pumps to pump liquid out of said volume at a second nominal rate;

means for monitoring the fluid pressure or volume within said volume during said controlling step; and

means for adjusting at least one of said nominal pump rates in response to said monitored fluid pressure or volume so as to obtain calibrated relative pump flow rates between plural pumps.

24. Apparatus for calibrating, during a preliminary set-up period, anticoagulant pump flow with respect to blood pump flow in a blood constituent processing system, said apparatus comprising:

disposable plastic tubing located in a blood constituent process system which includes a closed fluid flow path between an anticoagulant pump connected to a source of anticoagulant solution and

a blood pump connected to a source of saline solution;

means for pumping fluid into said path with one of said pumps at a first predetermined nominal rate and pumping fluid out of said path with the other of said pumps at a second predetermined nominal rate, which rates are initially set to be at assumed equal values;

means for detecting changes in fluid pressure within said path caused by said pumping;

means for adjusting at least one of said first and second rates in response to said detected changes so as to maintain an approximately constant fluid pressure within said path; and

means for deriving a relative pump flow calibration factor based on the controlled nominal flow rates required by said means for adjusting.

25. A method for automatically deriving relative flow calibration data for plural pumps connected with a common fluid path therebetween and a normally open fluid path which establishes fluid communication between the common fluid path and a fluid source, said method comprising:

establishing a closed fluid path which includes said common fluid path by terminating, during a preliminary set-up period, fluid communication between said common fluid path and said fluid source;

automatically controlling said pumps, during said preliminary set-up period, to inject fluid into said common fluid path and/or to withdraw fluid from said common fluid path at respectively associated nominal pumping rates;

automatically measuring changes in at least one fluid flow parameter occurring within said closed common fluid path in response to said controlling of said pumps at said respectively associated nominal rates;

and

automatically deriving said relative flow calibration data for the individual pumps in response to said measured changes.

26. A method of operating a fluid system of the type having plural pumps connected with a common fluid path therebetween and a normally open fluid path which establishes fluid communication between the common fluid path and a fluid source, said method comprising:



- (a) deriving relative flow calibration data for said plural pumps by:
  - (i) establishing a closed fluid path which includes said common fluid path by terminating, during a preliminary set-up period, fluid communication between said common fluid path and said fluid source;
  - (ii) automatically controlling said pumps, during said preliminary set-up period, to inject fluid into said common fluid path and/or to withdraw fluid from said common fluid path at respectively associated nominal pumping rates;
  - (iii) automatically measuring changes in at least one fluid flow parameter occurring within said closed common fluid path in response to said controlling of said pumps at said respectively associated nominal rate; and
  - (iv) automatically deriving said relative flow calibration data for the individual pumps in response to said measured changes; and then
- (b) reestablishing, during a normal operating cycle after said preliminary set-up period, said normally open fluid path and controlling the operating rates of said plural pumps based upon said derived relative flow calibration data.

27. Apparatus for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween and a normally open fluid path which establishes fluid communication between the common fluid path and a fluid source, said apparatus comprising:

means for establishing a closed fluid path which includes said common fluid path by terminating, during a preliminary set-up period, fluid communication

between said common fluid path and said fluid source;

means for automatically controlling said pumps, during said preliminary set-up period, to inject fluid into said common fluid path and/or to withdraw fluid from said common fluid path at respectively associated nominal pumping rates;

means for automatically measuring changes in at least one fluid flow parameter occurring within said closed common fluid path in response to said controlling of said pumps at said respectively associated nominal rates; and

means for automatically deriving said relative flow calibration data for the individual pumps in response to said measured changes.

28. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween, said method comprising the steps of:



automatically controlling said pumps to inject fluid into said common fluid path and/or to withdraw from said common fluid path at respectively associated nominal pumping rates;

automatically measuring changes in at least one fluid flow parameter occurring within said common fluid path in response to said controlling step of said pumps at said respectively associated nominal rates;

comparing said measured changes in said at least one flow parameter to a predetermined standard value for said flow parameter;

automatically continually modifying the pumping rate of at least one of said pumps from said nominal pumping rate thereof in response to said measured changes being at variance with said predetermined standard value until said measured changes are comparable to said predetermined standard value; and

automatically deriving relative calibration data representative of said modified pumping rate of said at least one pump relative to said respective nominal rate thereof, whereby calibration data for the individual pumps using said measured changes is obtained.

29. A method for deriving a relative flow calibration data for plural pumps connected with a common fluid path, said method comprising the steps of:



- (a) operating said pumps at respective nominal pumping rate such that one pump injects fluid into said path and another pump withdraws fluid from said path;
- (b) measuring changes of at least one fluid flow parameter occurring within said common fluid path during said operation of said pumps at said respective nominal pumping rates and determining whether said measured changes are within a predetermined value which is required to maintain an approximately constant fluid pressure in said path while said one pump is injecting fluid into said path and said another pump is withdrawing fluid from said path;
- (c) modifying the pumping rate of said one and/or another pumps from said nominal pumping rate thereof until said changes of said at least one fluid flow parameter measured according to step (b) is within said predetermined value; and
- (d) deriving a calibration value for said one and/or another pumps which is representative of said modified pumping rate, whereby calibration data for said pumps is obtained.

30. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path, said apparatus comprising:



means for controlling said pumps to inject fluid into said path and/or to withdraw fluid from said path at respectively associated nominal rates;

means for measuring changes in at least one fluid flow parameter occurring within said path in response to said injection of fluid into and withdrawal of fluid from said common fluid path; and

means for deriving relative flow calibration data for the individual pumps, said means for deriving including:

- (i) means for comparing said measured changes in said at least one flow parameter to a predetermined standard value for said flow parameter;
- (ii) means for automatically continually modifying the pumping rate of at least one of said pumps from said nominal pumping rate thereof in response to said measured changes being at variance with said predetermined standard value until said measured changes are comparable to said predetermined standard value; and
- (iii) means for generating a calibration value representative of said modified pumping rate of said at least one pump relative to said respective nominal rate thereof, whereby calibration data for the individual pumps using said measured changes is obtained.



31. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween as hereinbefore particularly described with reference to what is shown in Figs. 1 to 3.
32. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween as hereinbefore particularly described with reference to what is shown in Fig. 4.
33. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween as hereinbefore particularly described with reference to what is shown in Fig. 5.
34. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween as hereinbefore particularly described with reference to what is shown in Fig. 6.
35. A method for automatically deriving relative flow calibration data of plural pumps connected with a common fluid path therebetween as hereinbefore particularly described with reference to what is shown in Figs. 1, 2 and 7.
36. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path as hereinbefore particularly described with reference to what is shown in Figs. 1 to 3.



37. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path as hereinbefore particularly described with reference to what is shown in Fig. 4.

38. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path as hereinbefore particularly described with reference to what is shown in Fig. 5.

39. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path as hereinbefore particularly described with reference to what is shown in Fig. 6.

40. Apparatus for deriving relative flow calibration data for plural pumps connected with a common fluid path as hereinbefore particularly described with reference to what is shown in Figs. 1, 2 and 7.

Dated this 5th day of March 1990.

BAXTER INTERNATIONAL INC.,

Patent Attorneys for the Applicant:

PETER MAXWELL & ASSOCIATES.



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FIG. 1

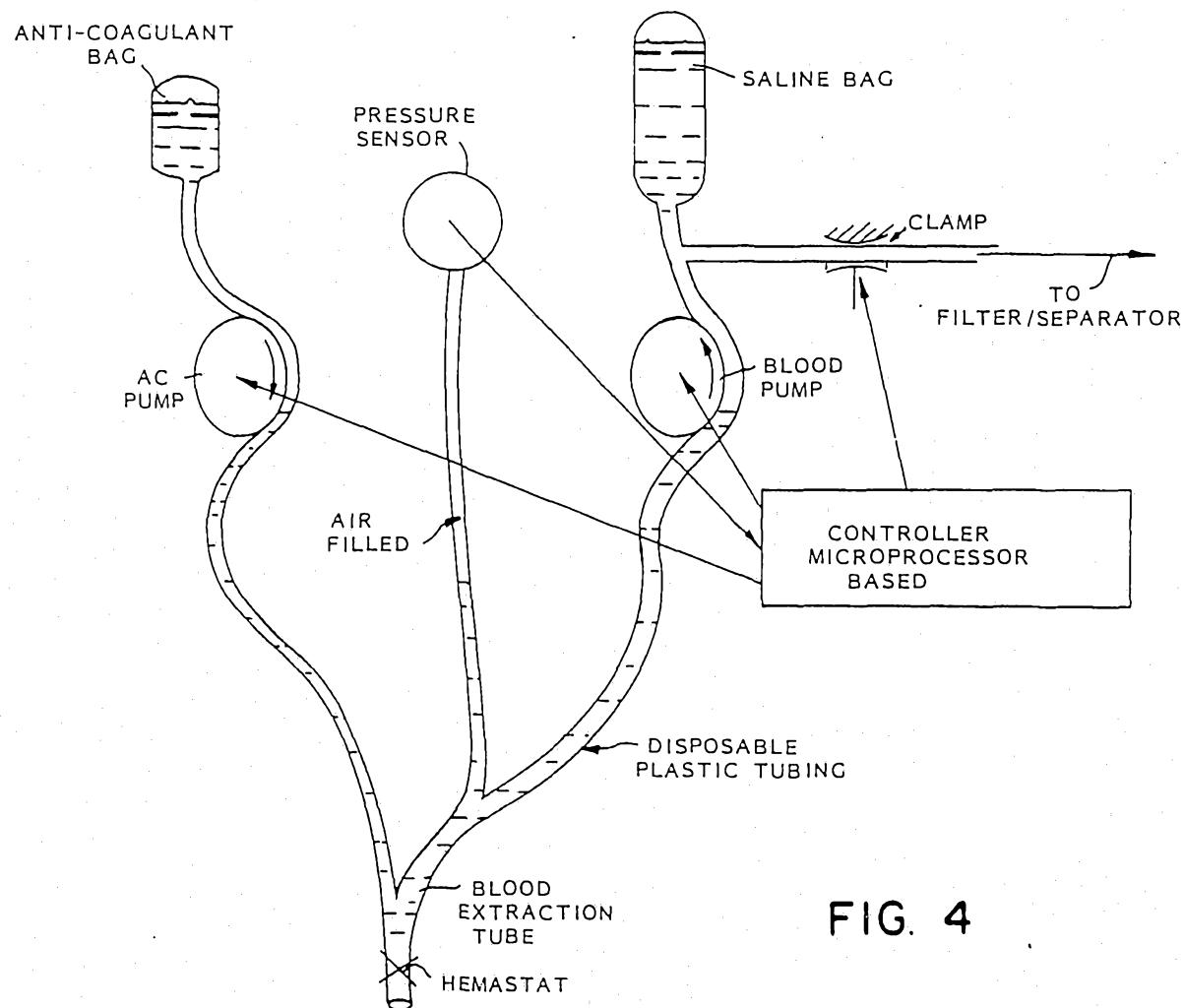
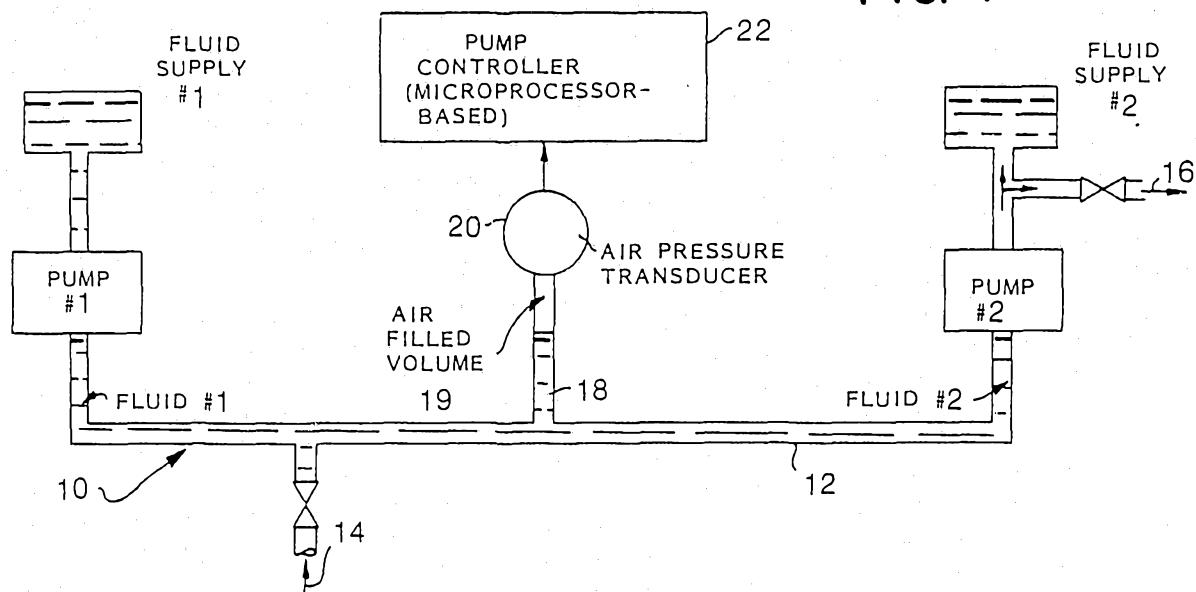
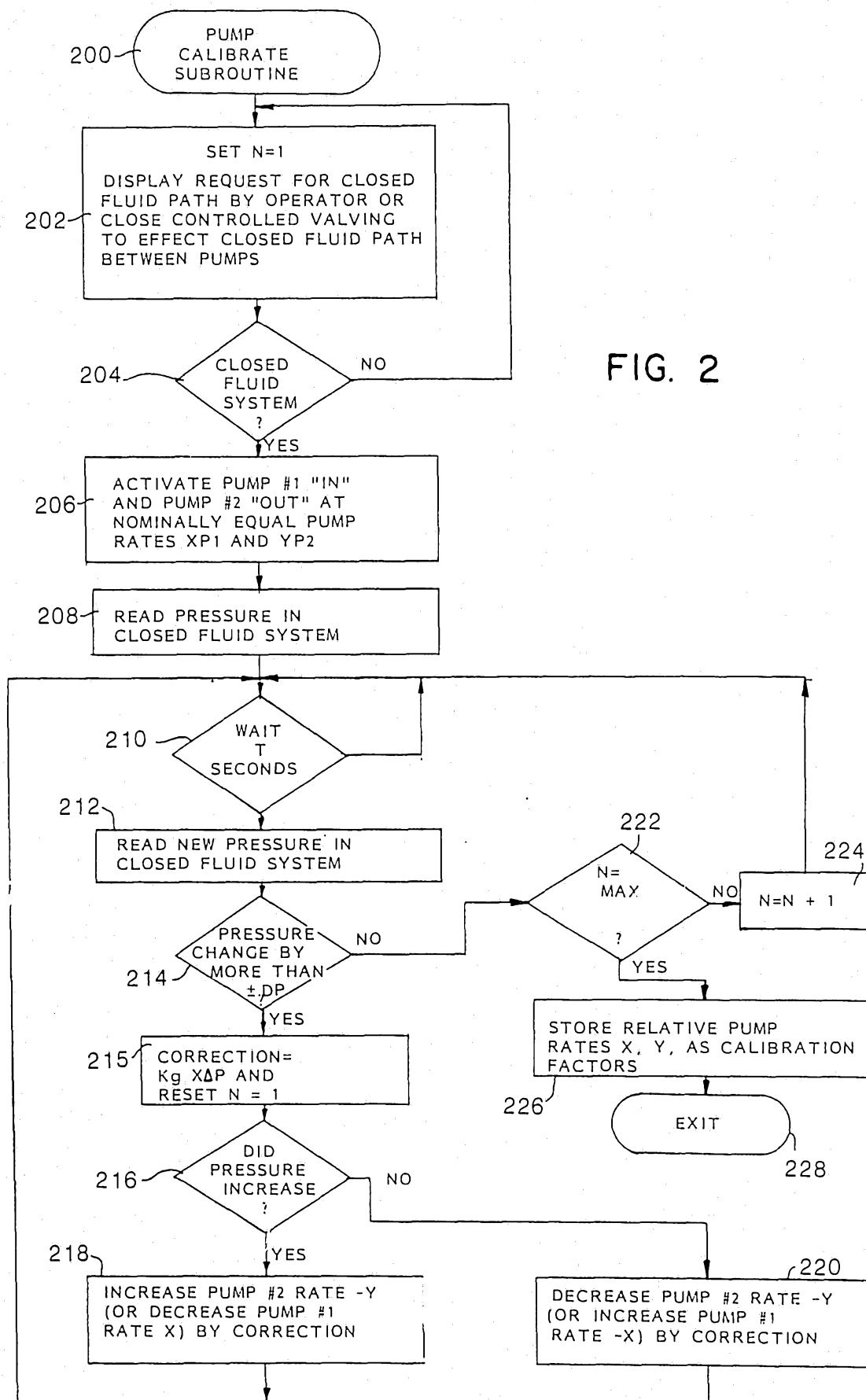


FIG. 4

**SUBSTITUTE SHEET**

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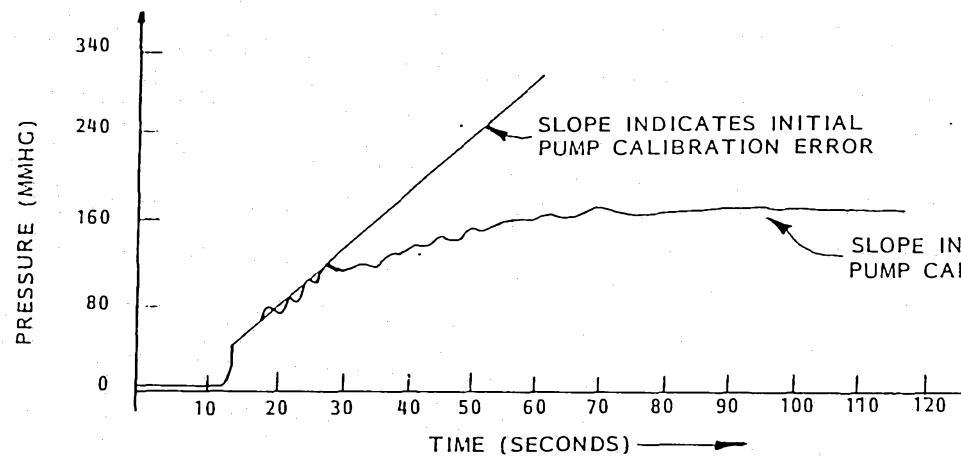
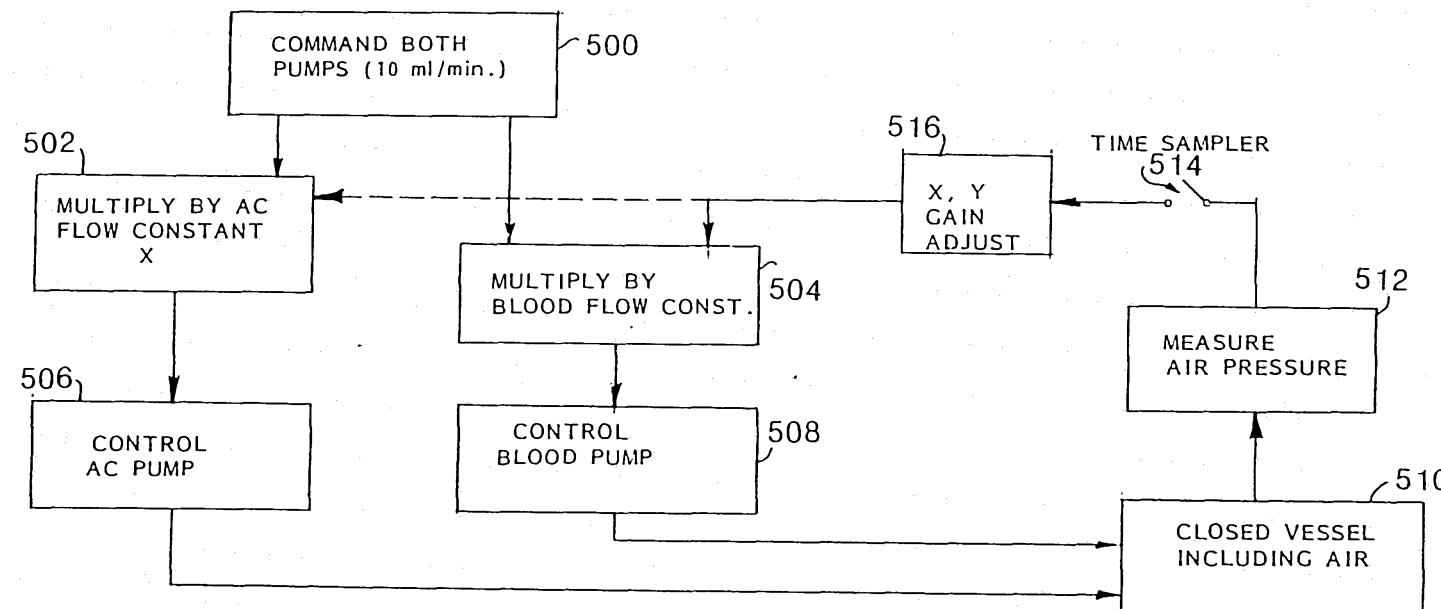


FIG. 3

FIG. 5

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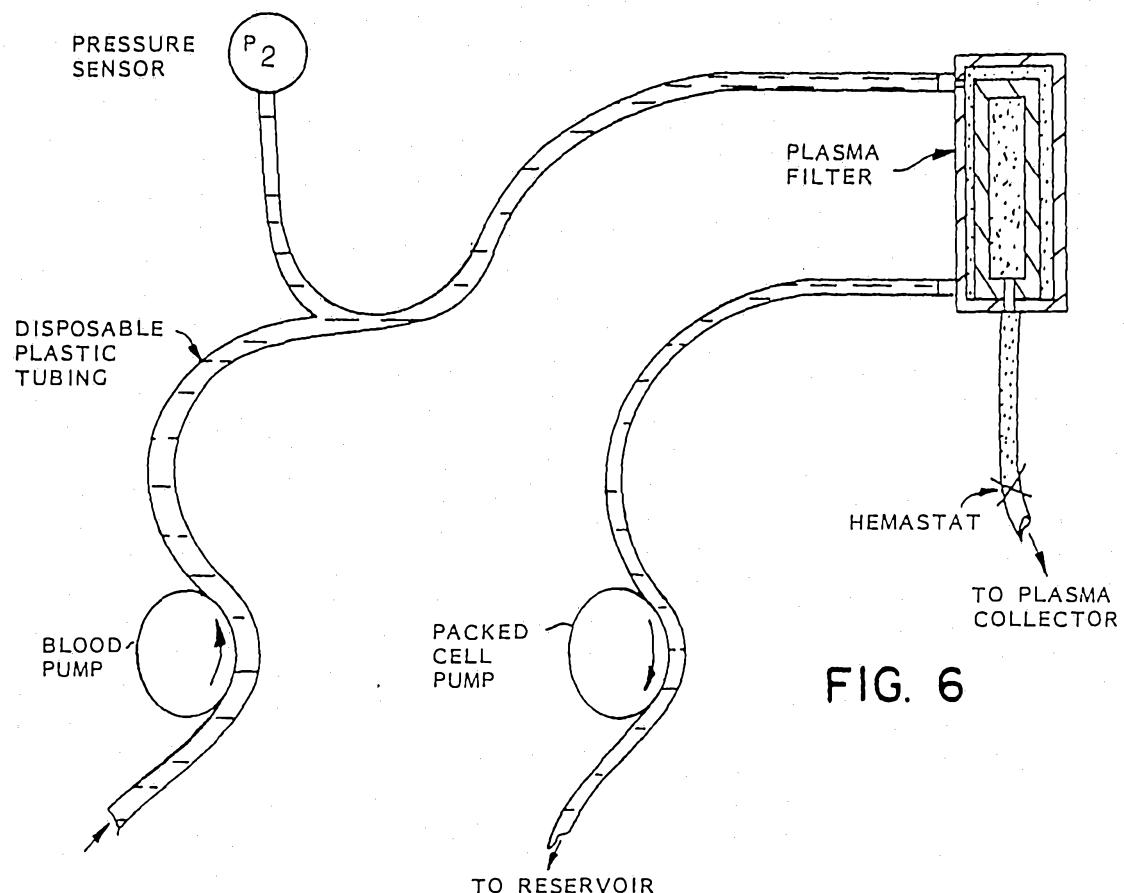
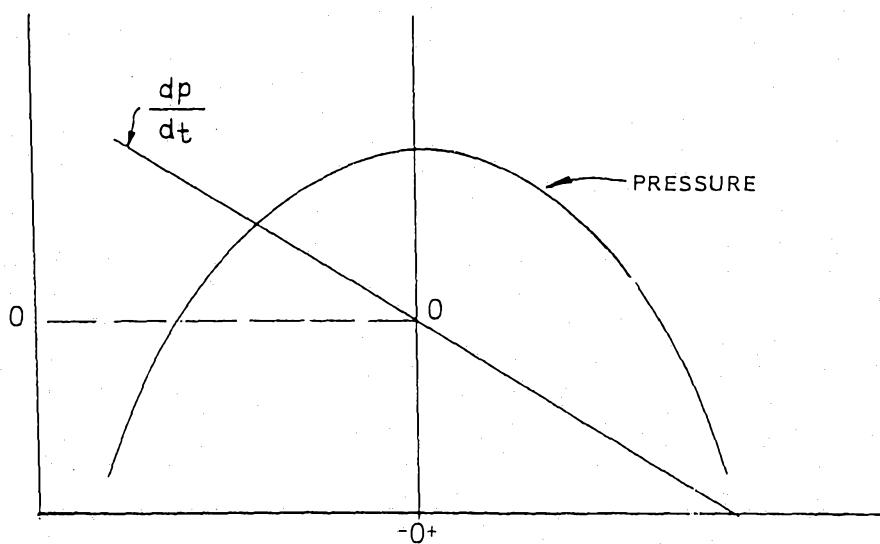


FIG. 6



RATE OF ERROR OF PACKED CELL PUMP RELATIVE TO BLOOD PUMP

FIG. 7

SUBSTITUTE SHEET

I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all) <sup>1</sup>

According to International Patent Classification (IPC) or to both National Classification and IPC

IPC(4): A61M 37/00

U.S. Cl. 604/4,6

## II. FIELDS SEARCHED

Minimum Documentation Searched <sup>4</sup>

| Classification System | Classification Symbols                      |
|-----------------------|---|
| U.S.                  | 604/4,5,6,67,82,131,151; 128 DIG 12, DIG 13 |

Documentation Searched other than Minimum Documentation  
to the Extent that such Documents are Included in the Fields Searched <sup>5</sup>III. DOCUMENTS CONSIDERED TO BE RELEVANT <sup>14</sup>

| Category <sup>6</sup> | Citation of Document, <sup>16</sup> with indication, where appropriate, of the relevant passages <sup>17</sup> | Relevant to Claim No. <sup>18</sup> |
|-----------------------|--|-------------------------------------|
| Y                     | US,A, 4,303,193 (LATHAM) 01 DECEMBER 1981<br>See entire document   | 1-24                                |
| Y                     | US,A, 4,197,847 (DJERASSI) 15 APRIL 1980<br>See entire document  | 1-24                                |
| Y                     | US,A, 4,086,924 (LATHAM) 02 MAY 1978<br>See entire document  | 1-24                                |
| A                     | US,A, 4,416,654 (SCHOENDORFER)<br>22 NOVEMBER 1983, See entire document  | 1-24                                |
| AT                    | US,A, 4,648,866 (MALBRANCQ) 10 MARCH 1987<br>See entire document   | 1-24                                |
| A                     | US,A, 4,563,173 (LEDLEY) 07 JANUARY 1986<br>See entire document  | 1-24                                |

<sup>6</sup> Special categories of cited documents: <sup>15</sup><sup>7</sup> "A" document defining the general state of the art which is not considered to be of particular relevance<sup>8</sup> "E" earlier document but published on or after the international filing date<sup>9</sup> "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)<sup>10</sup> "O" document referring to an oral disclosure, use, exhibition or other means<sup>11</sup> "P" document published prior to the international filing date but later than the priority date claimed<sup>12</sup> "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention<sup>13</sup> "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step<sup>14</sup> "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art<sup>15</sup> "&" document member of the same patent family

## IV. CERTIFICATION

Date of the Actual Completion of the International Search <sup>1</sup>

06 MAY 1987

Date of Mailing of this International Search Report <sup>1</sup>

22 MAY 1987

International Searching Authority <sup>1</sup>

ISA/US

Signature of Authorized <sup>19</sup>

John D. Ferros