



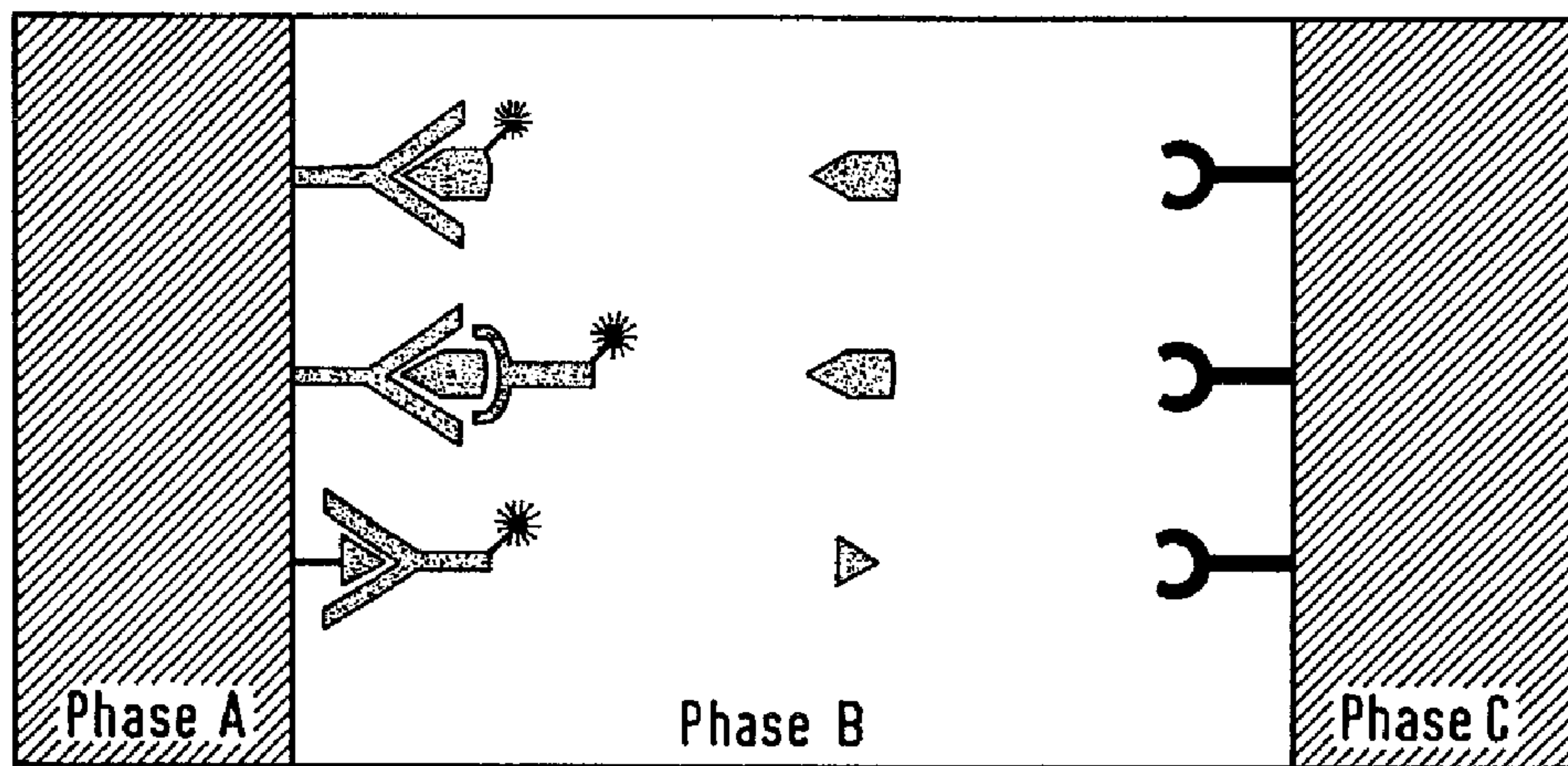
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(54) Titre : PROCÉDE DE MISE EN OEUVRE D'UN DOSAGE IMMUNOLOGIQUE DANS UN SYSTEME MULTIPHASE  
 (54) Title: METHOD OF CARRYING OUT AN IMMUNOASSAY IN A MULTIPHASE SYSTEM

## Assays in a multiphase system

### (1) Principle



Immune reaction

- Concentration
- Equilibrium displacement
- Signal alteration
- Signal generation
- Label protection

(57) Abrégé/Abstract:

The invention concerns a method of carrying out an immuno-assay in a multi-phase system.



**PCT**

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<p>(21) Internationales Aktenzeichen: PCT/EP95/02447 (22) Internationales Anmeldedatum: 23. Juni 1995 (23.06.95)  (30) Prioritätsdaten: P 44 21 907.5 24. Juni 1994 (24.06.94) DE  (71) Anmelder (für alle Bestimmungsstaaten ausser US): BEHRINGWERKE AKTIENGESELLSCHAFT [DE/DE]; Postfach 11 40, D-35001 Marburg (DE).  (72) Erfinder; und (75) Erfinder/Anmelder (nur für US): NEUENHOFER, Stephan [DE/DE]; Rotenberg 19, D-35037 Marburg (DE). KÄSMARKER, Reinhard [AT/DE]; Badener Strasse 6, D-65824 Schwalbach/Ts. (DE).</p>		<p>(81) Bestimmungsstaaten: AU, CA, JP, KR, MX, US, europäisches Patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).  <b>Veröffentlicht</b> <i>Mit internationalem Recherchenbericht. Vor Ablauf der für Änderungen der Ansprüche zugelassenen Frist. Veröffentlichung wird wiederholt falls Änderungen eintreffen.</i></p> <p style="text-align: center; font-size: 2em;">2193079</p>
<p>(54) Title: METHOD OF CARRYING OUT AN IMMUNO-ASSAY IN A MULTI-PHASE SYSTEM (54) Bezeichnung: VERFAHREN ZUR DURCHFÜHRUNG EINES IMMUNOASSAYS IN EINEM MEHRPHASENSYSTEM (57) Abstract The invention concerns a method of carrying out an immuno-assay in a multi-phase system. (57) Zusammenfassung Die vorliegende Erfindung betrifft ein Verfahren zur Durchführung eines Immunoassays in einem Mehrphasensystem.</p>		

Method for carrying out an immunoassay in a multiphase system

The present invention relates to a method for carrying  
5 out an immunoassay in a multiphase system.

Immunological detection methods have become very important in in vitro diagnostics. The reason for this is that they are highly specific and extremely sensitive.  
10 In addition, these assays are easy to implement. The detection methods are based on the immunological interaction between the analyte which is to be detected and its binding partner or partners.

15 In sandwich assays, the analyte is bound, as in a sandwich, by two different antibodies. One of the two antibodies carries a label (marker) which enables its concentration to be determined.

20 The sandwich method is not appropriate for small analytes since, for example for steric reasons, two different antibodies are not able to bind to the analyte simultaneously. As a rule, the competitive assays are used under these circumstances. In these  
25 assays, an analyte and a synthetic derivative of the analyte, for example, compete for the binding sites of the antibody. As a rule, either the analyte derivative (conventional competitive method) or the antibody (e.g. SPALT: solid phase antigen luminescence technique) is  
30 labeled. The labeled component is termed a tracer.

A disadvantage of the known competitive methods is that their sensitivity is relatively low as compared with that of sandwich assays since, in contrast to the  
35 situation in immunometric assays, the detection reagents cannot be employed in excess, and it is consequently not possible to displace the equilibrium

position to the extent desired in favor of the immune complex to be detected.

As a rule, it is necessary to separate off the excess  
5 free tracer antibody (in the case of sandwich assays and when carrying out SPALT) or the unbound analyte tracer (in the case of the conventional competitive method) before measuring the signal emitted by the label.

10

In the methods known as "homogeneous assays", a separation of this nature is not required since the signals from the free and bound tracers differ from each other.

15 Heterogeneous assays suffer from the disadvantage that, before measuring the signal which correlates with the analyte concentration, one or more separation steps are required in order to separate off the labeled immune complex, which is usually bound to a solid phase, from  
20 the free, labeled reagent. This additional step is relatively laborious when an assay is being carried out manually and increases the susceptibility of the method to error; even when carried out on automated analytical equipment, the step of separation is disadvantageous  
25 since an additional subassembly is generally required for this method step.

For this reason, "homogeneous assays" were developed at an early stage. The homogeneous assay, which is known  
30 under the designation EMIT (enzyme-multiplied immunoassay technology) (Biochem. Biophys. Res. Commun. 47: 846, 1972), has proved to be of value for detecting small molecules, for example of drugs (e.g. steroids). In a modified EMIT, the activity of the enzyme being  
35 used as label decreases when the analyte/enzyme conjugate binds to the antibody which is directed against the analyte. This is apparently due to a diminished affinity of the substrate for the active center of the enzyme in the presence of the antibody,

or to steric hindrance, or to a conformational change in the enzyme.

A further variant of EMIT is based on inhibition of the enzymic activity by the analyte derivative which is bound covalently to the enzyme. In this case, the activity is restored when the antibody which is directed against the analyte binds to the enzyme-labeled analyte derivative. Another variant of this method has been developed for relatively large analytes such as, for example, IgG (Anal. Biochem. 102: 167, 1990). However, the sensitivity which is achieved using this method is fairly low.

FETIA (fluorescence excitation transfer immunoassay; J. Biol. Chem. 251: 4172, 1976) is based on the transfer of energy between two fluorescent molecules, one of which is linked to the antibody while the other is linked to the analyte derivative. In this case, the analyte which is to be detected prevents formation of the complex between the labeled antibody and the labeled analyte derivative.

ECIA (enzyme channelling immunoassay; Anal. Biochem. 1056: 223, 1979; Appl. Biochem. Biotechnol. 6, 53-64, 1981) makes use of an antibody and of an analyte tracer each of which carries a different enzyme. The product of the first enzymic reaction constitutes the substrate for the second enzymic reaction. The overall velocity of the two reactions is markedly increased by this co-immobilization.

In SLFIA (substrate-labeled fluorescent immunoassay), an analyte derivative which is labeled with an enzyme substrate competes with the analyte for the binding sites of the anti-analyte antibody. Binding of the substrate-labeled analyte derivative to the antibody prevents the substrate from being reacted enzymically

(Burd J.F., Feeney J.E., Carrico R.J., Bogulaski R.C.: Clin. Chem. 23, 1402, 1977; Wong R.C., Burd J.F., Carrico R.J., Buckler R.T., Thoma J., Bogulaski R.C.: Clin. Chem. 25, 686, 1979).

5

If a fluorescent compound is excited in solution with polarized light, the emission which is observed is also polarized. The degree of this polarization depends on the mobility of the excited molecule. The decreasing mobility of a fluorescent tracer when the latter is bound to an antibody is used, in a fluorescence polarization immunoassay, to differentiate between free and bound tracer.

15 A fluorescence protection immunoassay (H.E. Ullmann: Tokai J. Exp. Clin. Med., Vol. 4, Supplement, pp. 7-32, 1979) is a homogeneous assay which operates in accordance with the competitive method.

In a conventional competitive assay, sufficient anti-analyte antibodies remain free, when analyte concentrations are low, for binding the tracer in such a manner that the label is no longer accessible to an anti-fluorescein antibody and can consequently no longer be quenched. This steric screening can be made even more effective by coupling the anti-analyte antibodies to a sterically demanding component.

In the solid phase antigen technique, the binding of an unwieldy analyte derivative to the tracer antibody prevents, in an analogous manner, its binding simultaneously to the anti-fluorescein antibody.

In a variant of the fluorescence protection immunoassay, the nonspecific absorption of light by active charcoal due to its coupling to the anti-fluorescein antibody is exploited to increase the quenching effect (scavenging effect).

Other techniques have been described, such as, for example, ALFPIA (antigen-labelled fluorescence protection assay; Clin. Chem. 25: 1077, 1979) or SPA (scintillation proximity assay; US patent 4,568,649; 5 WO 90/11524), in which a signal is generated by means of a radioactive tracer binding close to a scintillator.

The object underlying this invention was to provide an 10 improved method for carrying out an immunoassay, which method is superior to the known methods, particularly as regards sensitivity, lack of susceptibility to potentially interfering influences and implementation.

15 The object was achieved by employing, in the present novel method, besides the customary components of an immunoassay which is known from the state of the art, such as, for example, a receptor A which can, for example, be an antigen, an antigen derivative or an 20 antibody, and a tracer which can, independently of the test structure selected, be, for example, a labeled antibody or a labeled antigen, a receptor B as an additional component, which receptor is directed against the label and generates or qualitatively and/or 25 quantitatively alters a signal by interacting with the label. At the same time, suitable immobilization of receptors A and B on one or more phases ensures that the tracer cannot bind simultaneously to receptors A and B. This has the advantage that a tracer which is 30 bound to receptor A and a tracer which is not bound to receptor A can be differentiated directly since they elicit signals which are qualitatively and/or quantitatively different. As a result, it is possible to establish test systems which exhibit a higher 35 sensitivity, a decreased susceptibility to potentially interfering influences and improved implementation as compared to those systems which are known from the state of the art.

The present invention consequently relates to a method for determining an analyte, in which method a sample containing the analyte to be detected is brought into contact with a receptor A and a tracer so that the analyte either

10 a) forms a complex with the tracer, which complex can be detected by the label (immunometric principle), or

15 b) counteracts the formation of a complex of receptor A and tracer by competing with the tracer for binding to receptor A, which is directed against the analyte (competitive principle), or

20 c) counteracts the formation of a complex of receptor A and tracer by competing with receptor A, which is structurally identical to the analyte or structurally similar to the analyte (competitive principle),

25 which comprises additionally

1) adding a receptor B, which generates or qualitatively and/or quantitatively alters a signal by interacting with the label,

30 and

2) determining the signal brought about by the label,

35 with a suitable immobilization of receptors A and B on or in one phase or several phases ensuring that the tracer either cannot enter into any binding involving the simultaneous participation of receptors A and B or

can enter into such a binding to only such a slight extent that it is nevertheless possible to detect and differentiate differing analyte concentrations.

5 In the simplest case, receptor B is an antibody which is directed against the label. However, it is, of course, also possible, when label = enzyme, for receptor B to be an enzyme substrate or an enzyme inhibitor. It is likewise possible, for example, for  
10 the label to be a biotinylated enzyme and for receptor B to be an avidin or streptavidin which inhibits the catalytic activity of the enzyme by binding to the biotin residue. That which is always crucial is that the label and receptor B form a "pair" in the sense  
15 that their interaction results in the generation of a signal or an alteration to a signal.

Naturally, the positions of label and receptor B can also be switched. For example, the anti-analyte  
20 antibody would then, in the case of a SPALT assay, be conjugated to receptor B rather than, as is otherwise customary, labeled with the label, whereas the label is positioned such that only free (i.e. not bound to the solid phase-bound analyte (derivative)) conjugate of  
25 anti-analyte antibody and receptor B can bind to the label.

Within the scope of the present invention, a tracer is, in its most general form, understood to be a labeled  
30 receptor. In this context the label can be bound covalently or non-covalently to the receptor. All the tracers, and also receptors and labels, which are known from the state of the art can be employed in accordance with the invention provided that they are only combined  
35 with each other in a manner which is meaningful and with which the skilled person is familiar. The receptor moiety of the tracer can either be a single receptor or consist of two or more receptors which can in turn be

linked to each other either covalently or non-covalently.

5 A label is understood to mean a compound which is capable of emitting a signal or of directly or indirectly generating a signal; for example a luminogenic group or an enzyme.

10 In the case of a conventional competitive assay, the equilibrium of the analyte-specific immune reaction can, in the method described herein, be shifted in favor of the immune complexes to be detected using an additional, linked-in immune reaction. In the simplest case, this is achieved by the analyte displacing an  
15 analyte tracer from the binding site of an antibody A, and the analyte tracer, which has thus been "extracted" being bound by an antibody B in an additional immune reaction.

20 Whereas antibody A is directed against analyte and analyte tracer, antibody B is only able to bind the analyte tracer. As a result, the analyte tracer is no longer able to participate in the customary manner in the equilibrium reaction "antibody A/analyte/analyte  
25 tracer".

By virtue of this specificity, which is only directed against the analyte tracer, of antibody B, and by means of choosing a suitably high concentration of the  
30 antibody B, the position of the equilibrium can be influenced in a very favorable manner. This thereby reduces the disadvantages of a normal competitive immune reaction as regards sensitivity. If the signal emitted by the label is altered as a result of the  
35 tracer being bound to antibody B, there is then no need to separate off the component to be measured, since, in this case, the change in signal correlates with the concentration of the analyte to be determined. The

alteration of the emitted signal can either be elicited directly by the binding to antibody B or be elicited by the tracer being brought into a signal-modulating environment by means of the binding to antibody B. In the case of a fluorescence quenching effect, this can be achieved, for example, by conjugating antibody B with a quenching substance.

In the case of a sandwich assay, the number of sandwich complexes (composed of capturing antibody A, analyte and tracer antibody) which are formed correlates with the concentration of the analyte. Consequently, the remaining quantity of tracer which is not bound in the sandwich complex also correlates with the analyte concentration. This free tracer is bound by antibody B.

In the present invention, an appropriate immobilization of the two receptors A and B ensures that tracers are not able to enter into any stable immune complexes in which receptors A and B are participating simultaneously (for example sandwich complex composed of antibody A, analyte tracer and antibody B). One possibility for achieving this is to couple receptors A and B to different particles with the size and composition of the particles being chosen such that a binding of the tracer in which receptors A and B participate simultaneously is rendered more difficult or prevented. Furthermore, receptors A and B can also be bound to the same solid phase, but at a distance which is large enough to render more difficult or prevent such a binding to a tracer in which receptors A and B participate simultaneously.

In one embodiment, the invention provides a method for determining an analyte, in which method a sample containing the analyte to be detected is brought into contact with a

## 9a

receptor A and a tracer containing a luminogenic label so that the analyte either

a) forms a complex with the tracer, which complex can be detected by the label (immunometric principle), or

b) counteracts the formation of a complex of receptor A and tracer by competing with the tracer for binding to receptor A, which is directed against the analyte (competitive principle), or

c) counteracts the formation of a complex of receptor A and tracer by competing with receptor A, which is structurally identical to the analyte or structurally similar to the analyte (competitive principle),

which comprises additionally

1) adding a soluble receptor B, which generates or qualitatively and/or quantitatively alters a signal by interacting with the label,

and

2) determining the signal brought about by the label,

with a suitable immobilization of receptors A and B on or in one phase or several phases ensuring that the tracer either cannot enter into any binding involving the simultaneous participation of receptors A and B or can

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enter into such a binding to only such a slight extent that it is nevertheless possible to detect and differentiate differing analyte concentrations. In another embodiment, the invention provides the method in accordance with the competitive principle, wherein

- a) receptor A is directed against the analyte, and
- b) the tracer is a derivative of the analyte, against which derivative both receptor A and receptor B are directed.

In yet another embodiment, the invention provides a method in accordance with the competitive principle, wherein

- a) the tracer is a receptor which is directed against the analyte and receptor A, and
- b) receptor A is either structurally identical to the analyte or is a derivative of the analyte.

In another embodiment, the invention provides a method in accordance with the immunometric principle, wherein

- a) receptor A is directed against the analyte, and
- b) the tracer is a receptor which is directed against the analyte, which receptor is either directed against another epitope of the analyte than is receptor A or, if the analyte possesses several identical epitopes, recognizes another epitope or the same epitope as does receptor A.

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The receptors A and B may be bound to or in different phases. The two phases may be different gel layers. In another embodiment, the receptors A and B may be bound to or in the same phase. In yet another embodiment, at least one phase is an inner or outer surface of a solid body. The solid body may be a membrane, a small tube or a microtitration plate or a part thereof.

In an embodiment, the invention provides a method wherein at least one phase comprises a plastic surface. In another embodiment, at least one phase comprises one or more metal-containing and/or metal ion-containing plastic beads. In a further embodiment, at least one phase comprises one or more magnetizable plastic beads.

In one embodiment, the label is an acridinium ester, an acridinium acylsulfonamide, a luminol, an isoluminol or a derivative of these substances, a dioxetane, a luciferin, an oxalate or an oxalic amide. In another embodiment, the label is bound directly to the tracer. In yet another embodiment, the label is bound indirectly to the component which is to be labeled by way of a receptor which is directed against the component which is to be labeled.

In one embodiment, Receptor B is a monoclonal antibody, a polyclonal antibody, an antibody fragment, a chemically modified antibody or a chemically modified antibody fragment.

In a further embodiment, the label is an acridinium compound and the receptor B possesses a double helical DNA structure, the function of which comprises preventing, or rendering more difficult, the emission of light from the label which is bound by the receptor.

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In another embodiment of the invention, a receptor B' is also added, which receptor binds to the label and thereby brings about a signal change which is qualitatively and/or quantitatively different from that brought about by receptor B. In another embodiment, receptor B does not bring about any signal change.

In a further embodiment, after receptor A, the sample, the tracer and receptor B have been incubated, a liquid is added in order to decrease the sample proportion during the determination of the signal provoked by the label, or wherein, after receptor A, the sample and the tracer have been incubated, receptor B is added in a liquid volume which is greater than that of the sample which is used.

In yet another embodiment, in each case, receptor B is employed in place of the label and the label is employed in place of receptor B.

The invention also provides a method for determining an analyte, in which method a sample containing the analyte to be detected is brought into contact with a preformed complex composed of tracer containing a luminogenic label and receptor A, so that the analyte either

- a) displaces the tracer from the binding with receptor A, which is directed against the analyte, or
- b) displaces receptor A, which is structurally identical to the analyte or structurally similar to the analyte, from the binding with the tracer,

which comprises, in addition,

9e

1) adding a soluble receptor B which binds to the tracer,

2) and, after a separation step, determining the signal which is evoked by the complex composed of receptor A and tracer or receptor B and tracer,

with a suitable immobilization of receptors A and B on or in one phase or several phases ensuring that the tracer either cannot enter into any binding involving the simultaneous participation of receptors A and B or can enter into such a binding to only such a slight extent that it is nevertheless possible to detect and differentiate differing analyte concentrations.

#### **BRIEF DESCRIPTION OF THE DRAWINGS**

Figure 1 shows the basic principles of a multiphase assay system.

Figure 2 shows the OPUS assay.

Figure 3 shows the signal quench produced by anti-label antibodies.

Figure 4 shows homogeneous assays in a multiphase system.

Figure 5 shows additional examples of homogeneous assays in a multiphase system.

Figure 6 shows another example of a homogeneous assay in a multiphase system.

Figure 7 shows a variation of the assay of Figure 6.

Figures 8 and 8a show a standard curve of LIA for determining PSA and a diagram of the method.

Figures 9 and 9a show a standard curve of ILMA for determining PSA and a diagram of the method.

Figures 10 and 10a show a standard curve of SPALT assay for determining thyroxine and a diagram of the method.

Figures 11 and 11a show a standard curve of LIA for determining thryoxine and a diagram of the method.

Figures 12 and 12a show a standard curve of a variation of LIA for determining thryoxine and a diagram of the method.

Figures 13 and 13a show a standard curve of LIA for determining FT3 and a diagram of the method.

Figure 14 shows a standard curve of an ILMA for determining PSA.

Figure 15 shows a standard curve of an ILMA for determining PSA.

Figure 16 shows a standard curve of LIA for determining T3.

Figure 17 shows the structure of  $[C_{74}H_{88}I_3N_7O_{19}S]^+[CF_3CO_2]^-$ .

Figure 18 is a key for the figures.

By way of example, the principles of some possible options are depicted diagrammatically in Fig. 1.

Examples of such spatial arrangements are:

1. Attachment of antibody A and antibody B to different plastic beads, with the size or the mass of the beads being chosen to be so large such that it is impossible for two beads to be stably bridged by a bond in which antibody A and antibody B mutually participate or that, for steric reasons, it is impossible for sufficient antibody B-coated beads to bind to an antibody A-coated bead.

2. Attachment of antibody A to a plastic bead and attachment of antibody B to the internal wall of the reaction tube.

The following is an example of an option for implementing a heterogeneous assay:

Plastic beads, which are coated with immobilized antibody A (anti-analyte antibody) which has previously been saturated with analyte tracer, are added to a polystyrene tube which is coated with antibody B (= anti-label antibody). After adding the sample, containing the analyte, and incubation buffer, the suspension is incubated and the plastic beads are then removed. The signal remaining in the tube is measured.

3. Fixing of antibody A and antibody B in different gel phases of a test element, as is employed, for example, in the OPUS<sup>®</sup> system (from BDI, Westwood, MA, USA.) (Fig. 2).

3a. An OPUS test module is modified in the following manner: Anti-fluorescence label antibodies (B antibodies) are embedded in the top layer of agarose, the middle layer serves, as usual, as the optical filter, and immune complexes composed of anti-analyte antibody (antibody A) and fluorescence-labeled analyte tracer are embedded in the bottom layer.

Analytes from the sample which is loaded on displace the tracer molecules from the immune complexes; the tracers diffuse out of the bottom layer and are bound by the anti-fluorescence label antibodies in the top layer. The fluorescence signal of the bottom layer is measured. This results in a standard curve which declines as the analyte concentration increases.

3b. An OPUS test module is modified in the following manner: anti-fluorescence label antibodies (B antibodies) are embedded in the bottommost agarose layer, the middle layer serves, as usual, as the optical filter, and immune complexes composed of anti-analyte antibody (antibody A) and fluorescence-labeled analyte tracer are embedded in the top layer.

Analytes from the sample which is loaded on displace the tracer molecules from the immune complexes; the tracers diffuse into the bottom layer and are bound by the anti-fluorescence label antibodies. The fluorescence signal of the bottom layer is measured. This results in a standard curve which rises with increasing analyte concentration.

4. Attachment of antibody A and antibody B to membrane fibers, with the distance between antibody A and antibody B on a fiber ensuring that the two antibodies cannot simultaneously enter into a bond with a tracer.

If the binding of the tracer to the antibody B brings about a change in the signal which is emitted by the tracer, the assay can then be carried out in such a manner that a separation and/or washing step becomes superfluous. In this case, the change in the signal correlates with the concentration of the analyte to be determined. The change in the signal can be a qualitative signal change, for example a shift in the emission wavelength, and/or a quantitative signal

change, for example a signal quench. The latter is depicted in Fig. 3 using the example of an acridinium acylsulfonamide label.

- 5 If the label/anti-label antibody pair is replaced by an enzyme/enzyme substrate pair, a signal can then be generated instead of there being a change in signal.

10 The incubation (steps) can be carried out in a variety of ways; the choice of sequence is, as in the case of the heterogeneous implementation, part of the normal optimization work. Examples are:

1. A preformed complex composed of antibody A (bound to  
15 a solid phase) and analyte tracer is incubated with the sample which contains analyte. Antibody B (likewise bound to a solid phase) is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . The signal is measured  
20 after a time  $t_2$  (see top line in Fig. 4)

2. A preformed complex composed of analyte derivative (bound to a solid phase) and labeled antibody A (SPALT principle) is incubated with the sample-containing  
25 analyte. Antibody B (likewise bound to a solid phase) is either present from the beginning of this incubation or else is only added after the passage of a certain time  $t_1$ . The signal is measured after a time  $t_2$  (see middle line in Fig. 4).

30  
3. A preformed complex composed of antibody A (bound to a solid phase), analyte and tracer antibody, that is a preformed sandwich complex, is incubated with the sample containing analyte and with antibody B (likewise  
35 bound to a solid phase). A modified analyte can also be employed in place of the analyte in the preformed sandwich complex in order to destabilize the preformed

complex and thereby facilitate displacement of the tracer (see bottom line in Fig. 4).

4. Antibody A (bound to a solid phase), analyte tracer  
5 and sample containing analyte are incubated together. After the passage of a certain time  $t_1$ , antibody B (likewise bound to a solid phase) is added, and the signal is measured after the passage of a time  $t_2$  (see top line in Fig. 5).

10

5. The sample containing analyte, and the tracer anti-  
body, are incubated together and, after the passage of  
a certain time  $t_1$ , a preformed complex composed of  
antibody A (bound to a solid phase) and analyte is  
15 added. After the passage of a time  $t_2$ , antibody B  
(likewise bound to a solid phase) is added, and the  
signal is measured after a time  $t_3$  (see middle line in  
Fig. 5).

20 6. Antibody A (bound to a solid phase), the sample  
containing the analyte, and the tracer antibody, are  
incubated. Once the sandwich complexes have formed,  
antibody B (likewise bound to a solid phase) is added,  
as a result of which that portion of the tracer which  
25 is not bound in the sandwich complex becomes bound by  
antibody B (see bottom line in Fig. 5).

7. A preformed complex composed of antibody A (bound to  
a solid phase) and analyte or analyte derivative is  
30 incubated together with the sample containing the  
analyte and with an analyte tracer. That portion of the  
tracer which is not bound by antibody A becomes bound  
by antibody B.

35 On top of this, the implementation of the assay can be  
varied by linking an additional immune reaction between  
the tracer and an additional antibody B' into the  
immune reaction between the tracer and antibody B.

While the solid-phase-bound antibody B, for example, has the function of binding that free portion of the tracer which remains following or during the analyte-specific immune reaction, in order to protect the  
5 signal of this tracer portion from any change, the signal of the tracer involved in the analyte-specific bond can be selectively altered by adding an antibody B' which is not bound to a solid phase.

10 This additional incubation step can be of advantage for, in a manually executed assay for example, being able to control more precisely the time during which antibody B exerts its effect, and/or, by means of  
15 appropriately high concentrations of antibody B', bringing about a more rapid and/or more clearly pronounced change in signal, for example in cases in which the quantity of antibody B which is present or can be added is limited due to the fact that the antibody is bound to a solid phase.

20

Some relevant examples are listed below:

8. A preformed complex composed of antibody A (bound to a solid phase) and analyte tracer is incubated with the  
25 sample containing analyte. Antibody B (bound to a different solid phase) is either present from the beginning of this incubation or else is only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , an antibody B' is added and the signal is measured after a  
30 suitable time  $t_3$ .

9. A preformed complex composed of analyte derivative (bound to a solid phase) and labeled antibody A (SPALT principle) is incubated with the sample containing  
35 analyte. Antibody B (likewise bound to a solid phase) is either present from the beginning of this incubation or is only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , an antibody B' is added and the

signal is measured after a further incubation time  $t_3$  (see Fig. 6).

10. A preformed complex composed of antibody A (bound to a solid phase), analyte and tracer antibody, that is a preformed sandwich complex, is incubated with the sample containing analyte and with antibody B (likewise bound to a solid phase). Antibody B' is then added and the signal is measured.

10

11. Antibody A (bound to a solid phase), analyte tracer and sample containing analyte are incubated together. After the passage of a certain time  $t_1$ , antibody B (likewise bound to a solid phase) is added, and antibody B' is added after the passage of a time  $t_2$ . The signal is then measured.

12. The sample containing analyte, and tracer antibody, are incubated together and, after the passage of a certain time  $t_1$ , a preformed complex composed of antibody A (bound to a solid phase) and analyte is added. After the passage of a time  $t_2$ , antibody B (likewise bound to a solid phase) is added, and antibody B' is added after a time  $t_3$ . The signal is then measured.

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13. Antibody A (bound to a solid phase), the sample containing the analyte, and tracer antibody, are incubated. Once the sandwich complexes have been formed, antibody B (likewise bound to a solid phase) is added, as a result of which that portion of the tracer which is not bound in the sandwich complex becomes bound by antibody B. When antibody B' is added, this antibody binds to the tracer which is involved in the sandwich complex.

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If the label group of the tracer is an enzyme, antibody B can then be replaced by an enzyme substrate. In this

case, a signal is generated as a result of contact between tracer and enzyme substrate. In this case too, the signal which is generated correlates with the concentration of the analyte to be determined. Examples  
5 of this are:

14. A preformed complex composed of antibody A (bound to a solid phase) and analyte tracer (analyte derivative labeled with an enzyme) is incubated with  
10 the sample containing analyte. An enzyme substrate, which is immobilized on a different solid phase, is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , the signal is measured.

15  
15. A preformed complex composed of analyte derivative (bound to a solid phase) and enzyme-labeled antibody A (SPALT principle) is incubated with the sample containing analyte. An enzyme substrate, which is bound  
20 to a different solid phase, is either present from the beginning of this incubation or else is only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , the signal is measured.

25 16. A preformed complex composed of antibody A (bound to a solid phase), analyte and tracer antibody, that is a preformed sandwich complex, is incubated with the sample containing analyte and with an enzyme substrate (likewise bound to a solid phase).

30  
17. Antibody A (bound to a solid phase), analyte tracer and sample containing analyte are incubated together. After the passage of a certain time  $t_1$ , an enzyme substrate (likewise bound to a solid phase) is added, and  
35 the signal is measured after the passage of a time  $t_2$ .

18. The sample containing the analyte, and tracer antibody, are incubated together and, after the passage of

a certain time  $t_1$ , a preformed complex composed of antibody A (bound to a solid phase) and analyte is added. After the passage of a time  $t_2$ , an enzyme substrate (likewise bound to a solid phase) is added, and the signal is measured after a time  $t_3$ .

19. Antibody A (bound to a solid phase), the sample containing the analyte, and tracer antibody, are incubated. Once the sandwich complexes have been formed, an enzyme substrate B (likewise bound to a solid phase) is added, and, as a result, that portion of the tracer which is not bound in the sandwich complex is able to react with the enzyme substrate.

20. A preformed complex composed of antibody A (bound to a solid phase) and analyte tracer is incubated with the sample containing analyte. An antibody B (likewise bound to a solid phase), which is directed against the enzyme and diminishes or inhibits the enzymic activity, is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , an enzyme substrate is added and the signal is measured after a suitable time  $t_3$ .

21. A preformed complex composed of analyte derivative (bound to a solid phase) and enzyme-labeled antibody A (SPALT principle) is incubated with the sample containing analyte. The antibody B (likewise bound to a solid phase), which is directed against the enzyme, is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , an enzyme substrate is added and the signal is measured after a further incubation time  $t_3$ .

22. A preformed complex composed of antibody A (bound to a solid phase), analyte and tracer antibody, that is a preformed sandwich complex, is incubated with the sample containing analyte and with antibody B (directed

against the enzyme and likewise bound to a solid phase). An enzyme substrate is then added and the signal is measured.

5 23. Antibody A (bound to a solid phase), analyte tracer and sample containing analyte are incubated together. After the passage of a certain time  $t_1$ , antibody B (directed against the enzyme and likewise bound to a solid phase) is added, and an enzyme substrate is added  
10 after the passage of a time  $t_2$ . The signal is then measured.

24. The sample containing analyte, and tracer antibody, are incubated together, and, after the passage of a  
15 certain time  $t_1$ , a preformed complex composed of antibody A (bound to a solid phase) and analyte is added. After the passage of a time  $t_2$ , antibody B (directed against the enzyme and likewise bound to a solid phase) is added, and an enzyme substrate is added  
20 after a time  $t_3$ . The signal is then measured.

25. Antibody A (bound to a solid phase), the sample containing the analyte, and tracer antibody, are incubated. Once the sandwich complexes have been formed,  
25 antibody B (directed against the enzyme and likewise bound to a solid phase) is added, and, as a result, that portion of the tracer which is not bound in the sandwich complex becomes bound by antibody B. By means of adding an enzyme substrate, the tracer involved in  
30 the sandwich complex can generate a signal.

All the examples cited here can, of course, be implemented in a variant in which the positions of the label and of receptor B are interchanged. The following are  
35 examples of this:

26. A preformed complex composed of antibody A (bound to a solid phase) and an analyte derivative conjugated

with receptor B is incubated with the sample containing analyte. The label (likewise bound to a solid phase) is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ .

5 After a time  $t_2$ , the signal is measured.

27. A preformed complex composed of analyte derivative (bound to a solid phase) and an antibody A conjugated with antibody B (SPALT principle) is incubated with the  
10 sample containing analyte. The label (likewise bound to a solid phase) is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , the signal is measured.

15  
28. A preformed complex composed of antibody A (bound to a solid phase), analyte and anti-analyte antibody labeled with antibody B, that is a preformed sandwich complex, is incubated with the sample containing  
20 analyte and with the label (likewise bound to a solid phase).

29. Antibody A (bound to a solid phase), an analyte derivative conjugated with antibody B, and sample con-  
25 taining analyte, are incubated together. After the passage of a certain time  $t_1$ , the label (likewise bound to a solid phase) is added, and the signal is measured after the passage of a time  $t_2$ .

30  
30. The sample containing analyte, and an anti-analyte antibody conjugated with antibody B are incubated together and, after the passage of a certain time  $t_1$ , a preformed complex composed of antibody A (bound to a solid phase) and analyte is added. After the passage of  
35 a time  $t_2$ , the label (likewise bound to a solid phase) is added, and the signal is measured after a time  $t_3$ .

31. Antibody A (bound to a solid phase), the sample containing the analyte, and an anti-analyte antibody conjugated with antibody B are incubated. Once the sandwich complexes have been formed, the label  
5 (likewise bound to a solid phase) is added, and, as a result, that portion of anti-analyte antibody conjugated with antibody B which is not bound in the sandwich complex is enabled to bind the label.
- 10 32. A preformed complex composed of antibody A (bound to a solid phase) and analyte derivative labeled with enzyme substrate is incubated with the sample containing analyte. An enzyme, which is immobilized on a different solid phase, is either present from the  
15 beginning of this incubation or else only added after the passage of a certain time  $t_1$ . After a time  $t_2$ , the signal is measured.
- 20 33. A preformed complex composed of analyte derivative (bound to a solid phase) and enzyme-substrate-labeled antibody A (SPALT principle) is incubated with the sample containing analyte. An enzyme, which is bound to a different solid phase, is either present from the beginning of this incubation or else only added after the  
25 passage of a certain time  $t_1$ . After a time  $t_2$ , the signal is measured.
- 30 34. A preformed complex composed of antibody A (bound to a solid phase), analyte and enzyme-substrate-labeled anti-analyte antibody, that is a preformed sandwich complex, is incubated with the sample containing analyte and with an enzyme (likewise bound to a solid phase).
- 35 35. Antibody A (bound to a solid phase), an analyte derivative labeled with enzyme substrate, and sample containing analyte are incubated together. After the passage of a certain time  $t_1$ , an enzyme (likewise bound

to a solid phase) is added, and the signal is measured after the passage of a time  $t_2$ .

36. The sample containing analyte, and anti-analyte antibody which is labeled with enzyme substrate are incubated together, and, after the passage of a certain time  $t_1$ , a preformed complex composed of antibody A (bound to a solid phase) and analyte is added. After the passage of a time  $t_2$ , an enzyme (likewise bound to a solid phase) is added, and the signal is measured after a time  $t_3$ .

37. Antibody A (bound to a solid phase), the sample containing the analyte, and enzyme-substrate-labeled anti-analyte antibody are incubated. Once the sandwich complexes have been formed, an enzyme (likewise bound to a solid phase), is added, and, as a result, that portion of enzyme-substrate-labeled antibody which is not bound in the sandwich complex is enabled to react with the enzyme.

38. A preformed complex composed of antibody A (bound to a solid phase) and enzyme-substrate-labeled analyte derivative is incubated with the sample containing analyte. An antibody B which is directed against the enzyme substrate (inhibits or prevents enzymic conversion of the enzyme substrate by binding to it; antibody B likewise bound to a solid phase) is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . An enzyme is added after a time  $t_2$ , and the signal is measured after a suitable time  $t_3$ .

39. A preformed complex composed of analyte derivative (bound to a solid phase) and enzyme-substrate-labeled antibody A (SPALT principle) is incubated with the sample containing analyte. The antibody B (bound to a different solid phase) which is directed against the

enzyme substrate is either present from the beginning of this incubation or else only added after the passage of a certain time  $t_1$ . An enzyme is added after a time  $t_2$ , and the signal is measured after a further 5 incubation time  $t_3$  (see Fig. 7).

40. A preformed complex composed of antibody A (bound to a solid phase), analyte, and anti-analyte antibody which is labeled with enzyme substrate, that is a 10 preformed sandwich complex, is incubated with the sample containing analyte and with antibody B (directed against the enzyme substrate and likewise bound to a solid phase). An enzyme is then added and the signal is measured.

15. 41. Antibody A (bound to a solid phase), an analyte derivative which is labeled with enzyme substrate, and sample containing analyte are incubated together. After the passage of a certain time  $t_1$ , antibody B (directed 20 against the enzyme substrate and likewise bound to a solid phase) is added, and an enzyme is added after the passage of a time  $t_2$ . The signal is then measured.

42. The sample containing analyte, and anti-analyte 25 antibody which is labeled with enzyme substrate are incubated together and, after the passage of a certain time  $t_1$ , a preformed complex composed of antibody A (bound to a solid phase) and analyte is added. After the passage of a time  $t_2$ , antibody B (directed against 30 the enzyme substrate and likewise bound to a solid phase) is added, and an enzyme is added after a time  $t_3$ . The signal is then measured.

43. Antibody A (bound to a solid phase), the sample 35 containing the analyte, and enzyme-substrate-labeled anti-analyte antibody are incubated. Once the sandwich complexes have been formed, antibody B (directed against the enzyme substrate and likewise bound to a

solid phase) is added, and, as a result, that portion of enzyme-substrate-labeled antibody which is not bound in the sandwich complex becomes bound by antibody B. When an enzyme is added, the tracer involved in the sandwich complex can generate a signal.

The present invention is additionally described by the examples below, which are intended to further elucidate the invention while in no way restricting it, and by the patent claims.

#### Example 1)

#### Luminescence immunoassay (LIA) for determining PSA

#### Preparation of the reagents:

##### Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/40) were coated with a monoclonal anti-PSA antibody (BW 92-283/029; Behringwerke AG, Marburg) using the carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], Part 2, Methoden Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody per ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg per ml of storage buffer (50 mM 2-cyclohexylaminoethanesulfonic acid (CHES), 0.5 g of NaN<sub>3</sub>/l, 3 g of bovine serum albumin/l, pH 8.0).

##### Solid phase B:

Magnetic particles were coated, as in the case of solid phase A, with a monoclonal antibody which is directed against the acridinium N-acylsulfonamide label (EP-A-0 257 541 and EP-A-0 330 050) (BW 90-9/04; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH [German

Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2184).

5 Tracer:

A monoclonal anti-PSA antibody (BW 92-284/03, Behringwerke AG) was labeled with the acridinium N-acylsulfonamide label (EP-A-0 257 541 and EP-A-0 330 050) in a molar ratio of 1+1. The labeling was carried  
10 out in accordance with the NHS method, which is described in the literature (NHS = N-hydroxysuccinimide reactive group; A.K. Campbell, Chemiluminescence: Principles and Applications in Biology and Medicine, 1st edition, VCH/Horwood, Weinheim/Chichester, 1988, p.  
15 439). Gel permeation chromatography (Sephadex G 25) was used for the purification. The tracer was stored at a concentration of 300 ng/ml of tracer buffer (10 mM sodium acetate, 150 mM NaCl, 2 g of bovine serum albumin/l, 0.1% Mergal K9N, pH 5.0).

20

PSA standards:

The buffer in which PSA (prostate-specific antigen, Behringwerke AG) was dissolved had the following composition: 50 mM Tris, 150 mM NaCl, 0.05% NaN<sub>3</sub>, 0.01%  
25 Tween 20, 0.5 g of bovine IgG/l, 40 g of bovine serum albumin/l, 8 mg of Titriplex V/l, pH 7.6. The standard concentrations were 0, 50, 100, 200 and 400 ng/ml.

Preformed complex:

30 The preformed complex composed of anti-PSA antibody (bound to solid phase A) and PSA was formed as follows: 1 ml of the solid phase A suspension and 1 ml of PSA solution [20mg/ml (10mM phosphate buffer, pH 7.3, containing 1 g of bovine IgG/l and 0.5 g of sodium  
35 azide/l)] were incubated at 37°C for 30 minutes, and the particles were then washed 5 times with 1 ml of buffer (magnetic separation), and made up to a final volume of 1 ml.

**Assay implementation:**

10 ml of sample containing PSA were incubated at RT for 5 2 minutes with 10 ml of tracer. 10 ml of the preformed complex were then added, followed by 10 ml of solid phase B after a further 2 minutes. The sample was subsequently measured in a luminometer (Berilux<sup>®</sup> analyzer) (measuring time 1 s).

10

The results are depicted in Fig. 8 and the assay implementation is depicted schematically in Fig. 8a.

**Example 2)**15 **Immunoluminometric assay (ILMA) for determining PSA****Preparation of the reagents:**Solid phase A:

20 Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/40) were coated with a monoclonal anti-PSA antibody (BW 92-283/029; Behringwerke AG, Marburg) using the carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], Part II, 25 Methoden Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody per ml of suspension had a magnetic particle concentration of 10 30 mg/ml of storage buffer (50 mM CHES, 0.5 g of NaN<sub>3</sub>/l, 3 g of bovine serum albumin/l, pH 8.0).

Solid phase B:

35 Magnetic particles were coated, as in the case of solid phase A, with a monoclonal antibody which is directed against the acridinium N-acylsulfonamide label (EP-A-0 257 541 and EP-A-0 330 050) (BW 90-9/04; Behringwerke AG; deposited in the Deutsche Sammlung von

Mikroorganismen und Zellkulturen GmbH [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2184). The ready-to-use suspension had a magnetic  
5 particle concentration of 2.5 mg/ml of storage buffer (50 mM CHES, 0.5 g of  $\text{NaN}_3$ /l, 3 g of bovine serum albumin/l, pH 8.0).

Tracer:

10 A monoclonal anti-PSA antibody (BW 92-284/03, Behringwerke AG) was labeled with the acridinium-N-acetylsulfonamide label (EP-A-0 257 541 and EP-A-0 330 050) in a molar ratio of 1+0.5. The labeling was carried out in accordance with the NHS method, which is  
15 described in the literature (NHS = N-hydroxysuccinimide reactive group; A.K. Campbell, Chemiluminescence: Principles and Applications in Biology and Medicine, 1st edition, VCH/Horwood, Weinheim/Chichester, 1988, p. 439). Gel permeation chromatography (Sephadex G 25) was  
20 used for the purification. The tracer was stored at a concentration of 30 mg/ml of tracer buffer (10 mM sodium acetate, 150 mM NaCl, 2 g of bovine serum albumin/l, 0.1% Mergal K9N, pH 5.0).

25 PSA standards:

The buffer in which PSA (prostate-specific antigen, Behringwerke AG) was dissolved had the following composition: 50 mM Tris, 150 mM NaCl, 0.05%  $\text{NaN}_3$ , 0.01% Tween 20, 0.5 g of bovine IgG/l, 40 g of bovine serum  
30 albumin/l, 8 mg of Titriplex V/l, pH 7.6. The standard concentrations were 0, 0.2, 0.4, 0.8, 1.6, 3.1, 6.2 and 12.5 mg/ml.

Assay implementation:

35

10 ml of sample containing PSA were incubated at 37°C for 20 minutes together with 10 ml of tracer and 10 ml of solid phase A. 10 ml of solid phase B were then

added, and the mixture was measured for 1 s in a luminometer (Berilux<sup>®</sup> analyzer) after a further 15 minutes.

- 5 The results are depicted in Fig. 9 and the assay implementation is depicted schematically in Fig. 9a.

Example 3)

SPALT assay for determining thyroxine

10

Preparation of the reagents:

Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. 15 EM1-100/20) were coated with the protein/T3 conjugate which is used in Berilux T3 in accordance with the carbodiimide method [G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], Part II, Methoden Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 20 4th ed. 1952, Vol. XV/2, 1974]. The coating concentration was 0.3 mg of conjugate per ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg per ml of storage buffer (50 mM Tris/citrate 25 buffer, 0.5 g of NaN<sub>3</sub>/l, 3 g of bovine serum albumin/l, pH 7.0).

Solid phase B:

Magnetic particles from Rhone-Poulenc (Catalog No. 30 EM1-100/40) were coated with a monoclonal antibody, which is directed against the acridinium N-acetylsulfonamide label (EP-A-0 257 541 and EP-A-0 330 050) (BW 90-8/04; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen 35 GmbH, [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2184), in accordance with the carbodiimide method [G. Wendlberger et al., Synthese

von Peptiden [Synthesis of peptides], Part II, Methoden  
Org. Chem. [Methods of organic chemistry] (Houben-Weyl)  
4th ed. 1952, Vol. XV/2, 1974]. The coating  
concentration was 6 mg of antibody per ml of 10%  
5 magnetic particle suspension. The ready-to-use  
suspension had a magnetic particle concentration of  
2.5 mg/ml of storage buffer (50 mM CHES, 0.5 g of  
NaN<sub>3</sub>/l, 3 g of bovine serum albumin/l, pH 8.0).

10 Tracer:

A monoclonal anti-T4 antibody (BW 86-49/7/1,  
Behringwerke AG) was labeled with the acridinium N-  
acylsulfonamide label (EP-A-0 257 541 and EP-A-0 330  
050) in a molar ratio of 1+5. The labeling was carried  
15 out using the NHS method, which is described in the  
literature (NHS = N-hydroxysuccinimide reactive group;  
A.K. Campbell, Chemiluminescence: Principles and  
Applications in Biology and Medicine, 1st edition,  
VCH/Horwood, Weinheim/Chichester, 1988, p. 439). Gel  
20 permeation chromatography (Sephadex G 25) was used for  
the purification. The tracer was stored at a concen-  
tration of 40 mg/ml of tracer buffer (50 mM citric  
acid/phosphate buffer, 2 g of polyethylene glycol  
6000/l, 2 g of Mowiol/l; pH 6.3).

25

T4 standards:

The buffer for the T4 standards had the following  
composition: 10 mM phosphate, 1 g of bovine IgG/l,  
0.5 g of NaN<sub>3</sub>/l; pH 7.3. The standard concentrations  
30 were 0, 0.1, 0.5, 1, 5, 10 and 50 mg/ml.

Preformed complex:

The preformed complex (tracer bound to solid phase A)  
was prepared as follows:  
35 6 ml of solid phase A were concentrated down to 3 ml  
(magnetic separation of the solid phase and  
resuspension in buffer). 0.2 ml of tracer was then  
added, and the mixture was incubated at 37°C for 30

minutes. The particles were washed 5 times with 10 mM phosphate buffer, 1 g of IgG/l, 0.5 g of NaN<sub>3</sub>/l, pH 7.3 (washing buffer). The particles were stored in 3 ml of washing buffer.

5

**Assay implementation:**

10 ml of sample containing T<sub>4</sub> were incubated at RT for 2 minutes with 10 ml of preformed complex. 10 ml of solid phase B were then added, and the mixture was measured for 1 s in a luminometer (Berilux<sup>®</sup> analyzer) after a further 2 minutes.

The results are depicted in Fig. 10 and the assay implementation is depicted schematically in Fig. 10a.

15

**Example 4)**

LIA for determining thyroxine (protector/quencher method)

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**Preparation of the reagents:**Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/20) were coated with a monoclonal anti-T<sub>4</sub> antibody (BW 86-49/7/1, Behringwerke AG) in accordance with the carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], Part II, Methoden Org. Chem. [Methods of organic chemistry], (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 1.2 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 1 g of bovine IgG/l, pH 8.0).

30

35

Solid phase B:

Magnetic particles from Rhône-Poulenc (Catalog No. EMI-100/40) were coated with a monoclonal antibody which is directed against the acridinium N-acylsulfonamide label (EP-A-0 257 541 and EP-A-0 330 050) (protector antibody, BW 90-9/016; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH, [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2183) in accordance with the carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of Peptides], Part II, Methoden. Org. Chem. [Methods of Organic Chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 3 g of bovine serum albumin/l, pH 8.0).

20 Tracer:

The tracer used in the Berilux FT3 was stored at a concentration of 360 ng/ml of tracer buffer (10 mM phosphate buffer, 1 g of IgG/l, pH 7.3).

25 Quencher antibody:

30 The anti-label antibody BW 90-8/04 (Behringwerke AG deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH, [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2184) was stored at a concentration of 0.1 mg/ml of buffer (10 mM phosphate, 1 g of IgG/l, 0.5 g of sodium azide/l, pH 7.3).

35 T4 standards:

BeriLux® T4 standards (Behringwerke AG) having a concentration of 0; 18; 40; 85; 175 and 340 ng/ml of serum medium were employed.

5 Preformed complex:

The preformed complex (tracer bound to solid phase A) was prepared as follows:

2 ml of tracer were added to 2 ml of solid phase A, and the mixture was incubated at 37°C for 30 minutes. The  
10 particles were washed 5 times with 10 mM phosphate buffer, 1 g of IgG/l, 0.5 g of sodium azide/l, pH 7.3, and were made up to 2 ml. 2 mg of ANS (8-anilinonaphthalene-1-sulfonic acid) were then added.

15 Assay implementation:

10 ml of preformed complex and 10 ml of sample containing T4 were incubated for 15 minutes. 10 ml of solid phase B and 10 ml of quencher antibody were  
20 subsequently added at intervals of in each case 10 minutes, and the suspension was measured for 1 s in a luminometer (BeriLux® analyzer).

A constant incubation temperature of 37°C was maintained.

25

The results are depicted in Fig. 11 and the assay implementation is depicted schematically in Fig. 11a.

Example 5)

30 LIA for determining thyroxine

Preparation of the reagents:

Solid phase A:

35 Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/20) were coated with a monoclonal anti-T4 antibody (BW 86-49/7/1, Behringwerke AG) in accordance with the carbodiimide method (G. Wendlberger et al., Synthese

von Peptiden, [Synthesis of peptides], Part II, Methoden Org. Chem. [Methods of organic chemistry], (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 1.25 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 1 g of bovine IgG/l, pH 8.0).

10 Solid phase B:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/40) were coated with a monoclonal antibody which is directed against the BeriLux label (Quencher antibody BW 90-8/04; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH, [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2184) in accordance with the carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], part II, Methoden Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 3 g of bovine serum albumin/l, pH 8.0).

Tracer:

30 The tracer used in the BeriLux FT3 was stored at a concentration of 360 ng/ml of tracer buffer (10 mM phosphate buffer, 1 g of IgG/l, 0.5 g of NaN<sub>3</sub>/l, pH 7.3).

35 T4 Standards:

BeriLux® T4 standards (Behringwerke AG) having a concentration of 0; 18; 40; 85; 175 and 340 ng/ml of serum medium were employed.

Preformed complex:

The preformed complex (tracer bound to solid phase A) was prepared as follows:

5 2 ml of tracer were added to 2 ml of solid phase A, and the mixture was incubated at 37°C for 30 minutes. The particles were washed 5 x with 10 mM phosphate buffer, 1 g of IgG/l, 0.5 g of sodium azide/l, pH 7.3, and were made up to 2 ml. 2 mg of ANS (8-anilidonaphthalene-1-  
10 sulfonic acid) were then added.

Assay implementation:

10 µl of preformed complex and 10 µl of sample  
15 containing T4 were incubated for 15 minutes. 10 µl of solid phase B were subsequently added and the mixture was incubated for a further 10 minutes before the suspension was measured for 1 s in a luminometer (Berilux® analyzer).

20 A constant incubation temperature of 37°C was maintained.

The results are depicted in Fig. 12 and the assay implementation is depicted schematically in Fig. 12a.

25 Example 6)

LIA for determining FT3

Preparation of the reagents:

30 Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/20) were coated with a monoclonal anti-T3 antibody (Berilux FT3 antibody) in accordance with the carbodiimide method (G. Wendlberger et al., Synthese  
35 von Peptiden, [Synthesis of peptides], Part II, Methoden Org. Chem. [Methods of organic chemistry], (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 0.25 mg of antibody/ml of 10%

magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 1 g of bovine IgG/l, pH 8.0).

5

Solid phase B:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/40) were coated with a monoclonal antibody which is directed against the Berilux label (Quencher antibody  
10 BW 90-8/04; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH, [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC : 2184) in accordance with the  
15 carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], part II, Methoden Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody/ml of 10% magnetic  
20 particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 3 g of bovine serum albumin/l, pH 8.0).

25 Tracer:

1 ng of hapten tracer (T3-acridinium tracer; see Fig. 17)/ml of tracer buffer (50 mM Tris/HCl; 150 mM NaCl; 0.5 mg of sodium azide/l; 0.1 g of Tween 20/l; 0.5 g of bovine IgG/l; 40 g of bovine serum albumin/l; 8 mg of  
30 Titriplex V/l; pH 7.6).

FT3 Standards:

FT3 standards in a concentration range of from 0 to 22 pg/ml were employed in a serum medium.

35

Assay implementation:

50  $\mu$ l of sample were incubated for 15 minutes together with 10  $\mu$ l of tracer and 10  $\mu$ l of solid phase A. 10  $\mu$ l of solid phase B were subsequently added and the mixture was incubated for a further 10 minutes before measuring the suspension for 1 s in a luminometer (Berilux® analyzer). A constant incubation temperature of 37°C was maintained.

The results are depicted in Fig. 13, and the assay implementation is depicted schematically in Fig. 13a.

#### Example 7)

#### Immunoluminometric assay (ILMA) for determining PSA

#### 15 Preparation of the reagents:

##### Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/40) were coated with a monoclonal anti-PSA antibody (BW 92-283/029; Behringwerke AG, Marburg) in accordance with the carbodiimide method (G. Wendlberger, P. Stelzel, Synthese von Peptiden, [Synthesis of peptides], Part II, Methoden Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 10 mg/ml of storage buffer (50mM CHES, 0.5 g of NaN<sub>3</sub>/l, 3 g of bovine serum albumin/l, pH 8.0).

##### Solid phase B:

Magnetic particles were, as in the case of solid phase A, coated with a monoclonal antibody which is directed against the Berilux label (BW 90-8/04; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH, [German Collection of Microorganisms and Cell Cultures], Braunschweig,

Germany, under deposition number DSM ACC 2184). The ready-to-use suspension had a magnetic particle concentration of 5 mg/ml of storage buffer (50 mM CHES, 0.5 g of  $\text{NaN}_3$ /l, 3 g of bovine serum albumin/l, pH 8.0).

5

Tracer concentrate:

A monoclonal anti-PSA antibody (BW 92-284/03, Behringwerke AG) was labeled with the Berilux® label in a molar ratio of 1 + 10. The labeling was carried out using the NHS method which is described in the literature (NHS = N-hydroxysuccinimide reactive group; A.K. Campbell, Chemiluminescence: Principles and Applications in Biology and Medicine, 1st edition, VCH/Horwood, Weinheim/Chichester, 1988, p. 439). Purification was effected by means of gel permeation chromatography (Sephadex G 25). The tracer was stored at a concentration of 30  $\mu\text{g/ml}$  of tracer buffer (10 mM sodium acetate, 150 mM NaCl, 2 g of bovine serum albumin/l, 0.1% Mergal K9N, pH 5.0).

15  
20

Tracer:

In order to prepare the ready-to-use tracer, the tracer concentrate is diluted, in a ratio of 1:200, with 0.1 M phosphate buffer (pH 6.3 containing 0.15 NaCl and 1 g of bovine serum albumin per liter).

25

PSA Standards:

The buffer in which the PSA (prostate-specific antigen, Behringwerke AG) was dissolved had the following composition: 50 mM Tris, 150 mM NaCl, 0.05%  $\text{NaN}_3$ , 0.01% Tween 20, 0.5 g of bovine IgG/l, 40 g of bovine serum albumin/l, 8 mg of Titriplex V/l, pH 7.6. The standard concentrations were 0, 0.5, 3.2, 10.6, 32, 80 and 160 ng/ml.

30  
35

Assay implementation:

10  $\mu$ l of PSA-containing sample were incubated at 37°C  
for 15 minutes together with 10  $\mu$ l of solid phase A and  
20  $\mu$ l of tracer. 10  $\mu$ l of solid phase B were  
subsequently added and, after a further 5 minutes, the  
5 mixture was measured for 0.7 s in a luminometer  
(Berilux® analyzer). 20 mM HNO<sub>3</sub> containing 0.5% H<sub>2</sub>O<sub>2</sub>  
and 125 mM NaOH were used as light emitting reagents.

The results are depicted in Fig. 14, and the assay  
10 implementation is depicted schematically in Fig. 9a.

#### Example 8)

#### Immunoluminometric assay (ILMA) for determining PSA

#### 15 Preparation of the reagents:

##### Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-  
100/40) were coated with a monoclonal anti-PSA antibody  
20 (BW 92-283/029; Behringwerke AG, Marburg) in accordance  
with the carbodiimide method (G. Wendlberger, P.  
Stelzel, Synthese von Peptiden, [Synthesis of  
peptides], Part II, Methoden Org. Chem. [Methods of  
organic Chemistry] (Houben-Weyl) 4th ed. 1952, Vol.  
25 XV/2, 1974). The coating concentration was 6 mg of  
antibody/ml of 10% magnetic particle suspension. The  
ready-to-use suspension had a magnetic particle  
concentration of 10 mg/ml of storage buffer (50mM CHES,  
0.5 g of NaN<sub>3</sub>/l, 3 g of bovine serum albumin/l, pH  
30 8.0).

##### Solid phase B:

Magnetic particles were, as in the case of solid phase  
A, coated with a monoclonal antibody which is directed  
35 against the Berilux label (BW 90-8/04; Behringwerke AG;  
deposited in the Deutsche Sammlung von Mikroorganismen  
und Zellkulturen GmbH, [German Collection of  
Microorganisms and Cell Cultures], Braunschweig,

Germany, under deposition number DSM ACC 2184). The ready-to-use suspension had a magnetic particle concentration of 5 mg/ml of storage buffer (50 mM CHES, 0.5 g of  $\text{NaN}_3$ /l, 3 g of bovine serum albumin/l, pH 8.0).

5

Tracer concentrate:

A monoclonal anti-PSA antibody (BW 92-284/03, Behringwerke AG) was labeled with the Berilux® label in a molar ratio of 1 + 10. The labeling was carried out using the NHS method which is described in the literature (NHS = N-hydroxysuccinimide reactive group; A.K. Campbell, Chemiluminescence: Principles and Applications in Biology and Medicine, 1st edition, VCH/Horwood, Weinheim/Chichester, 1988, p. 439). Purification was effected by means of gel permeation chromatography (Sephadex G 25). The tracer was stored at a concentration of 30 µg/ml of tracer buffer (10 mM sodium acetate, 150 mM NaCl, 2 g of bovine serum albumin/l, 0.1% Mergal K9N, pH 5.0).

15  
20

Tracer:

In order to prepare the ready-to-use tracer, the tracer concentrate is diluted, in a ratio of 1:200, with 0.1 M phosphate buffer (pH 6.3 containing 0.15 NaCl and 1 g of bovine serum albumin per liter).

25

Measuring buffer:

12.1 g of tris(hydroxymethyl)aminomethane, 8.8 g of sodium chloride, 0.1 g of sodium azide and 10 g of Tween 20 are dissolved in 990 ml of deionized water, and this solution is adjusted to pH 8.0 with 25% hydrochloric acid.

30

Medium effects can be reduced by employing the measuring buffer in combination with suitable light-emitting reagents (see assay implementation).

35

PSA Standards:

The buffer in which PSA (prostate-specific antigen, Behringwerke AG) was dissolved had the following composition: 50 mM Tris, 150 mM NaCl, 0.05% NaN<sub>3</sub>, 0.01% Tween 20, 0.5 g of bovine IgG/l, 40 g of bovine serum albumin/l and 8 mg of Titriplex V/l, pH 7.6. The standard concentrations were 0, 3.2, 10.6, 32, 80 and 160 ng/ml.

#### Assay implementation:

10

10 µl of PSA-containing sample were incubated at 37°C for 15 minutes together with 10 µl of solid phase A and 20 µl of tracer. 10 µl of solid phase B were subsequently added, as were 200 µl of measuring buffer after a further 5 minutes. The mixture was measured for 0.7 s in a luminometer (BeriLux® analyzer). 20 mM HNO<sub>3</sub> containing 0.5% H<sub>2</sub>O<sub>2</sub> and 125 mM NaOH were used as light-emitting reagents.

20 The results are depicted in Fig. 15, and the assay implementation is depicted schematically in Fig. 9a.

#### Example 9)

##### LIA for determining T3

25

##### Preparation of the reagents:

##### Solid phase A:

Magnetic particles from Rhône-Poulenc (Catalog No. EM1-30 100/20) were coated with a monoclonal anti-T3 antibody (BeriLux FT3-antibody) in accordance with the carbodiimide method [G. Wendlberger, P. Stelzel, Synthese von Peptiden, [Synthesis of peptides], Part II, Methoden Org. Chem. [Methods of organic chemistry] 35 (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974]. The coating concentration was 0.25 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of

2.5 mg/ml of storage buffer (10.36 g of CHES, 0.5 g of sodium azide, 3 g of bovine serum albumin/l, pH 8.0).

**Solid phase B:**

5 Magnetic particles from Rhône-Poulenc (Catalog No. EM1-100/60) were coated with a monoclonal antibody which is directed against the BeriLux label (Quencher antibody BW 90-8/04; Behringwerke AG; deposited in the Deutsche Sammlung von Mikroorganismen und Zellkulturen GmbH,  
10 [German Collection of Microorganisms and Cell Cultures], Braunschweig, Germany, under deposition number DSM ACC 2184) in accordance with the carbodiimide method (G. Wendlberger et al., Synthese von Peptiden [Synthesis of peptides], part II, Methoden  
15 Org. Chem. [Methods of organic chemistry] (Houben-Weyl) 4th ed. 1952, Vol. XV/2, 1974). The coating concentration was 6 mg of antibody/ml of 10% magnetic particle suspension. The ready-to-use suspension had a magnetic particle concentration of 2.5 mg/ml of storage  
20 buffer (10.36 g of CHES, 0.5 g of sodium azide, 3 g of bovine serum albumin per liter, pH 8.0).

**Synthesis of the tracer**

Step 1: Preparation of a streptavidin-T3 conjugate

25 a) 3 mg of streptavidin are dissolved in 1.7 ml of 0.1 M Na tetraborate buffer (containing 10% dioxane), pH 8.0. 28 µl of GMBS solution (5 mg of N-succinimidyl γ-maleimidobutyrate/ml of dioxane) are added. After the mixture has reacted at RT for 1 hour, it is rebuffered  
30 in 0.1 M phosphate buffer (contains 5mM EDTA), pH 6.0, by means of a PD10/G25m column. The resulting eluate ("solution 1") has a volume of 2 ml and a concentration of 0.9 mg of streptavidin/ml.

b) 7mg of triiodothyronine (T3) are dissolved in 700 µl  
35 of DMSO. 10 µl of N-ethylmorpholine and 1.6 mg of SAMSA (S-acetylmercaptosuccinic anhydride), dissolved in 80 µl of DMSO, are added. After 30 minutes, 100 µl of a 1 M aqueous solution of hydroxylamine are pipetted in. The

resulting solution ("solution 2") is incubated at RT for 15 minutes.

c) 1.76 ml of solution 1 and 41.5  $\mu$ l of solution 2 are mixed and left to stand at RT for 1 hour. Rebuffering in 0.1 M K phosphate buffer, pH 7.2, ("solution 3") subsequently takes place by means of a PD10/G25m column. After the rebuffering, the concentration of streptavidin-T3 conjugate is 0.6 mg/ml.

10 Step 2: Labeling of the streptavidin-T3 conjugate with Berilux label

a) Synthesis of the Berilux label having a biotin group:

200 mg (0.26 mmol) of Berilux label (possessing an NHS-reactive group) are initially introduced into 30 ml of acetonitrile, and a solution of 98 mg (0.26 mmol) of N-biotin-1,8-diamino-3,6-dioxaoctane (Boehringer Mannheim) and 46  $\mu$ l (0.3 mmol) of triethylamine in 5 ml of acetonitrile is added dropwise at RT; the reaction mixture is then stirred at RT for 12 h, during which time it becomes green in color. The mixture is filtered and the solvent is distilled off in vacuo. The residue (400 mg; green oil) is purified by preparative medium pressure chromatography (Büchi system) on a reversed-phase column [stationary phase: LichroPrep C-18 (from Merck); mobile phase: gradient of acetonitrile/water = 33:67 + 0.1% by vol of trifluoroacetic acid after acetonitrile/water = 45:55 + 0.1% by vol of trifluoroacetic acid]. 170 mg of a yellow powder are isolated after distilling off the acetonitrile in vacuo and removing the water by freeze drying. MS (FAB): [C<sub>47</sub>H<sub>55</sub>N<sub>6</sub>O<sub>9</sub>S<sub>2</sub>]<sup>+</sup> (calculated: 911.347; - found: 911.350) [CF<sub>3</sub>CO<sub>2</sub>]<sup>-</sup> (113).

b) 182  $\mu$ l of solution 3 (0.1 mg of streptavidin-T3 conjugate), 718  $\mu$ l of 0.1 M K phosphate buffer, pH 7.2, 14  $\mu$ l of acetonitrile and 86  $\mu$ l of a labeling solution [10 mg of Berilux label (possessing a biotin group)/ml of acetonitrile] are pipetted together and incubated at

RT for 30 minutes. The tracer is purified by gel chromatography through PD10/G25m.

**Preparation of the tracer solution**

5 6 ng of tracer/ml of tracer buffer  
tracer buffer: 100 mM PBS, pH 6.3, containing 0.2% bovine IgG, 0.1% Mergal and 0.025% ANS.

**T3 Standards:**

10 T3 standards were employed in a serum medium in a concentration range of from 0 to 7.5 ng/ml.

**Measuring buffer:**

100 mM Tris buffer, pH 8.0, containing 150 mM NaCl, 1%  
15 Tween 20 and 0.01% sodium azide.

**Assay implementation:**

50  $\mu$ l of sample were incubated at 37°C for 30 minutes together with 100  $\mu$ l of tracer and 20  $\mu$ l of solid phase  
20 A. 10  $\mu$ l of solid phase B were subsequently added, and 200  $\mu$ l of measuring buffer were pipetted in after the mixture had been incubated at RT for 10 minutes. The suspension was measured for 1 s in a luminometer (Berilux® analyzer) (emitting reagents: R1 = 20 mM  
25 nitric acid containing 0.5% hydrogen peroxide; R2 = 125 mM sodium hydroxide).

The results are depicted in Fig. 16 and the assay implementation is depicted schematically in Fig. 13a.

30

**Legend to Fig. 3**

The figure shows the quenching effect of three different anti-label antibodies on a tracer antibody which is labeled with a Berilux® label (acridinium acylsulfonamide label) (signal activity without adding  
35 an anti-label antibody = 100%).

Whereas the antibody BW 90-9/016 is particularly suitable for protecting the label from signal-altering

reagents, BW 90-8/04 can be employed as a signal-altering (in this case, signal-quenching) antibody. BW 89-191/019 is less well suited for either of these applications.

- 5 The measuring time in the BeriLux® analyzer is 1 second.

**Patent claims**

1. A method for determining an analyte, in which method a sample containing the analyte to be detected is brought into contact with a receptor A and a tracer containing a luminogenic label so that the analyte either

a) forms a complex with the tracer, which complex can be detected by the label, or

b) counteracts the formation of a complex of receptor A and tracer by competing with the tracer for binding to receptor A, which is directed against the analyte, or

c) counteracts the formation of a complex of receptor A and tracer by competing with receptor A, which is structurally identical to the analyte or structurally similar to the analyte,

which comprises additionally

1) adding a soluble receptor B, which generates or qualitatively and/or quantitatively alters a signal by interacting with the label,

and

2) determining the signal brought about by the label,

with an immobilization of receptors A and B on or in one phase or several phases ensuring that the tracer either cannot enter into any binding involving the simultaneous participation of receptors A and B or can enter into such a binding to only such a slight extent that it is nevertheless possible to detect and differentiate differing analyte concentrations.

2. The method as claimed in claim 1 in accordance with steps (b) or (c), wherein
  - a) receptor A is directed against the analyte, and
  - b) the tracer is a derivative of the analyte, against which derivative both receptor A and receptor B are directed.
3. The method as claimed in claim 1 in accordance with steps (b) or (c), wherein
  - a) the tracer is a receptor which is directed against the analyte and receptor A, and
  - b) receptor A is either structurally identical to the analyte or is a derivative of the analyte.
4. The method as claimed in claim 1 in accordance with step (a), wherein
  - a) receptor A is directed against the analyte, and
  - b) the tracer is a receptor which is directed against the analyte, which receptor is either directed against another epitope of the analyte than is receptor A or, if the analyte possesses several identical epitopes, recognizes another epitope or the same epitope as does receptor A.
5. The method as claimed in any one of claims 1-4, wherein the receptors A and B are bound to or in different phases.
6. The method as claimed in any one of claims 1-5, wherein the receptors A and B are bound to or in the same phase.

7. The method as claimed in any one of claims 1-6, wherein at least one phase is an inner or outer surface of a solid body.
8. The method as claimed in claim 7, wherein the solid body is a membrane, a small tube or a microtitration plate or a part thereof.
9. The method as claimed in any one of claims 1-8, wherein at least one phase comprises a plastic surface.
10. The method as claimed in any one of claims 1-9, wherein at least one phase comprises one or more metal-containing and/or metal ion-containing plastic beads.
11. The method as claimed in any one of claims 1-10, wherein at least one phase comprises one or more magnetizable plastic beads.
12. The method as claimed in claim 5, wherein the two phases are different gel layers.
13. The method as claimed in any one of claims 1-12, wherein the label is an acridinium ester, an acridinium acyl-sulfonamide, a luminol, an isoluminol or a derivative of these substances, a dioxetane, a luciferin, an oxalate or an oxalic amide.
14. The method as claimed in any one of claims 1-13, wherein the label is bound directly to the tracer.
15. The method as claimed in any one of claims 1-14, wherein the label is bound indirectly to the component which is to be labeled by way of a receptor which is directed against the component which is to be labeled.
16. The method as claimed in any one of claims 1-15, wherein the receptor B is a monoclonal antibody, a polyclonal

- antibody, an antibody fragment, a chemically modified antibody or a chemically modified antibody fragment.
17. The method as claimed in any one of claims 1-16, wherein the label is an acridinium compound and the receptor B possesses a double helical DNA structure, the function of which comprises preventing, or rendering more difficult, the emission of light from the label which is bound by the receptor.
  18. The method as claimed in any one of claims 1-17, wherein a receptor B' is also added, which receptor binds to the label and thereby brings about a signal change which is qualitatively and/or quantitatively different from that brought about by receptor B.
  19. The method as claimed in claim 18, wherein receptor B does not bring about any signal change.
  20. The method as claimed in any one of claims 1-19, wherein, after receptor A, the sample, the tracer and receptor B have been incubated, a liquid is added in order to decrease the sample proportion during the determination of the signal provoked by the label, or wherein, after receptor A, the sample and the tracer have been incubated, receptor B is added in a liquid volume which is greater than that of the sample which is used.
  21. The method as claimed in any one of claims 1-20, wherein, in each case, receptor B is employed in place of the label and the label is employed in place of receptor B.
  22. A method for determining an analyte, in which method a sample containing the analyte to be detected is brought into contact with a preformed complex composed of tracer containing a luminogenic label and receptor A, so that the analyte either

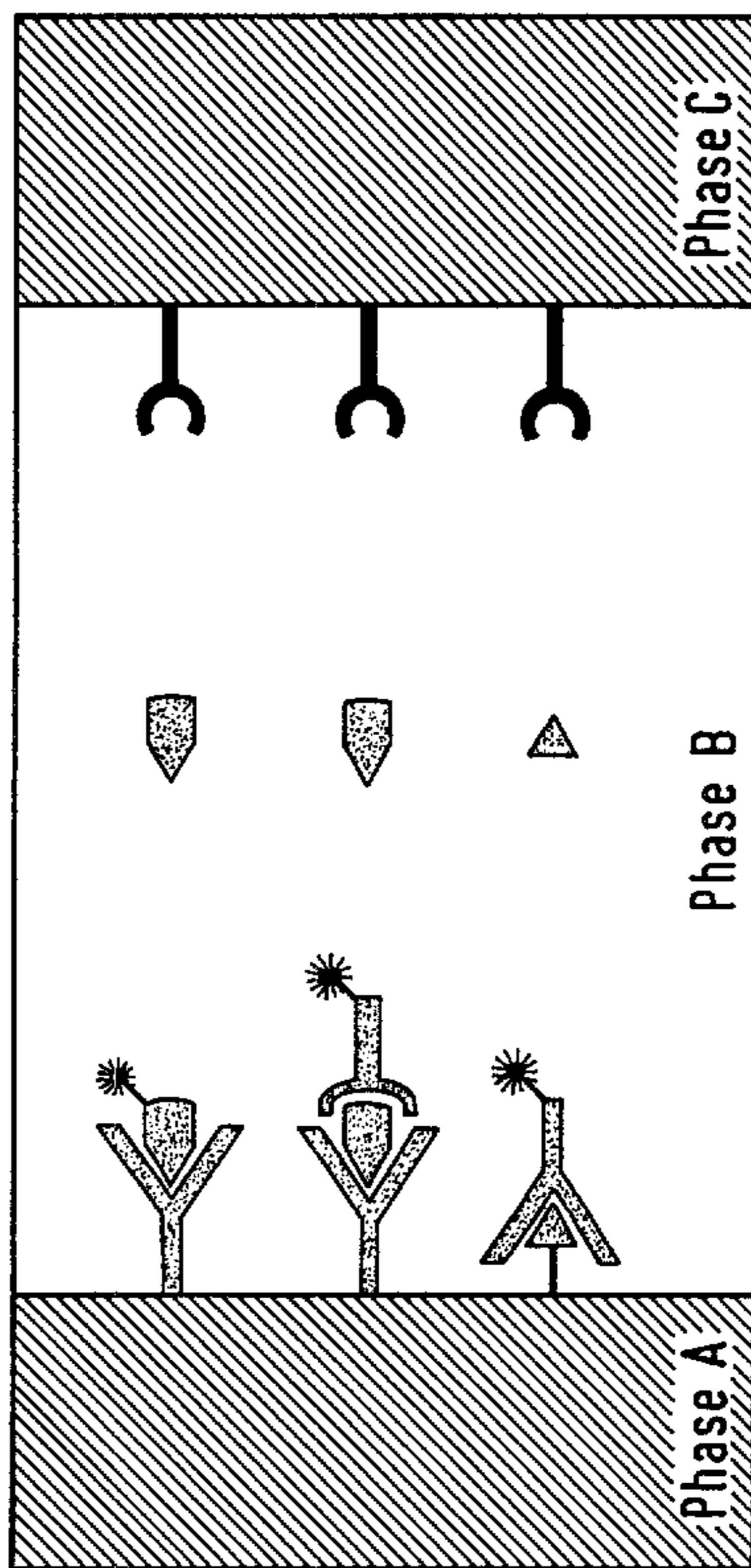
- a) displaces the tracer from the binding with receptor A, which is directed against the analyte, or
- b) displaces receptor A, which is structurally identical to the analyte or structurally similar to the analyte, from the binding with the tracer,

which comprises, in addition,

- 1) adding a soluble receptor B which binds to the tracer,
- 2) and, after a separation step, determining the signal which is evoked by the complex composed of receptor A and tracer or receptor B and tracer,

with an immobilization of receptors A and B on or in one phase or several phases ensuring that the tracer either cannot enter into any binding involving the simultaneous participation of receptors A and B or can enter into such a binding to only such a slight extent that it is nevertheless possible to detect and differentiate differing analyte concentrations.

FIG.1 Assays in a multiphase system  
(1) Principle



- Concentration
- Equilibrium displacement
- Signal alteration
- Signal generation
- Label protection

FIG.2 Assays in a multiphase system

(2) Example: OPUS

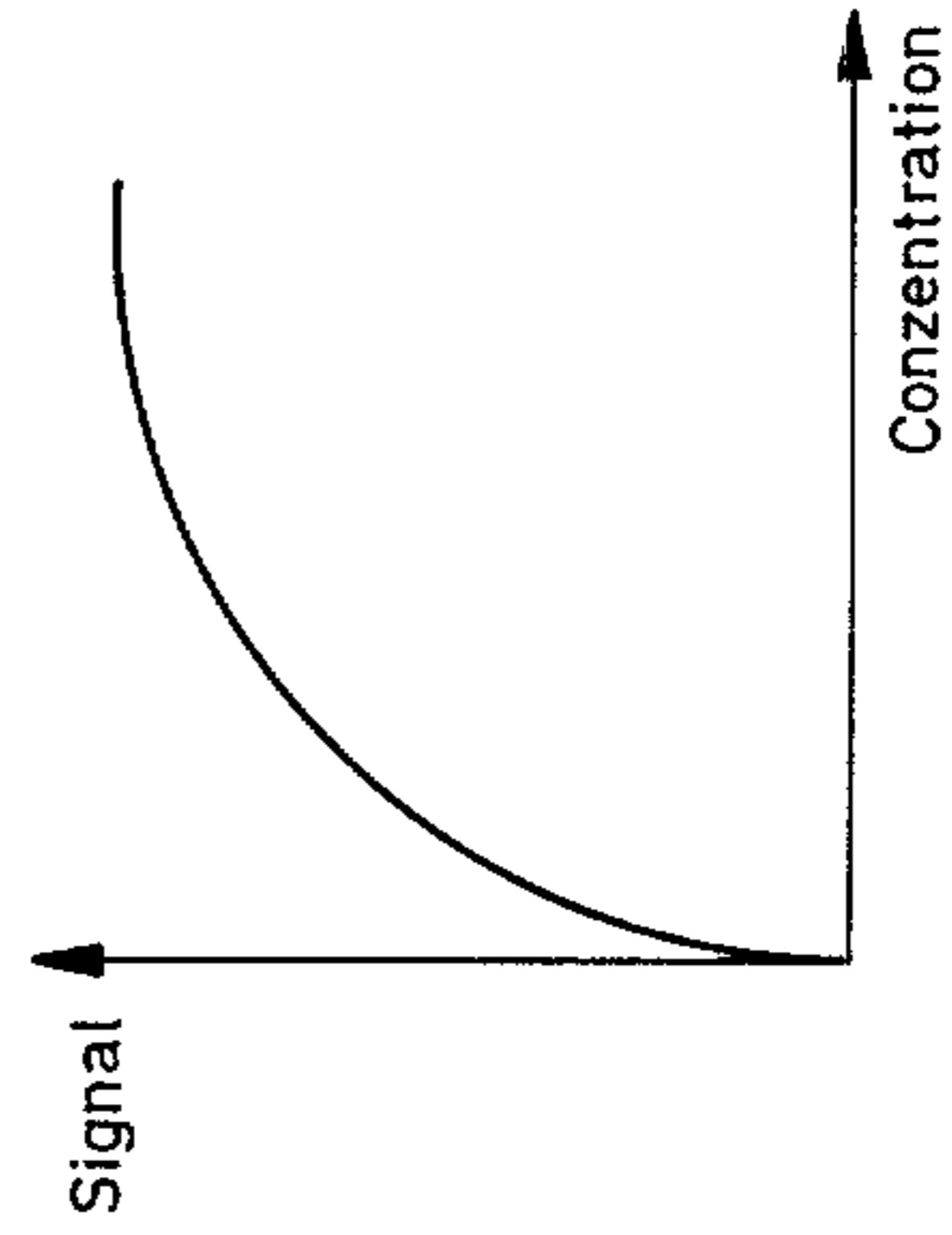
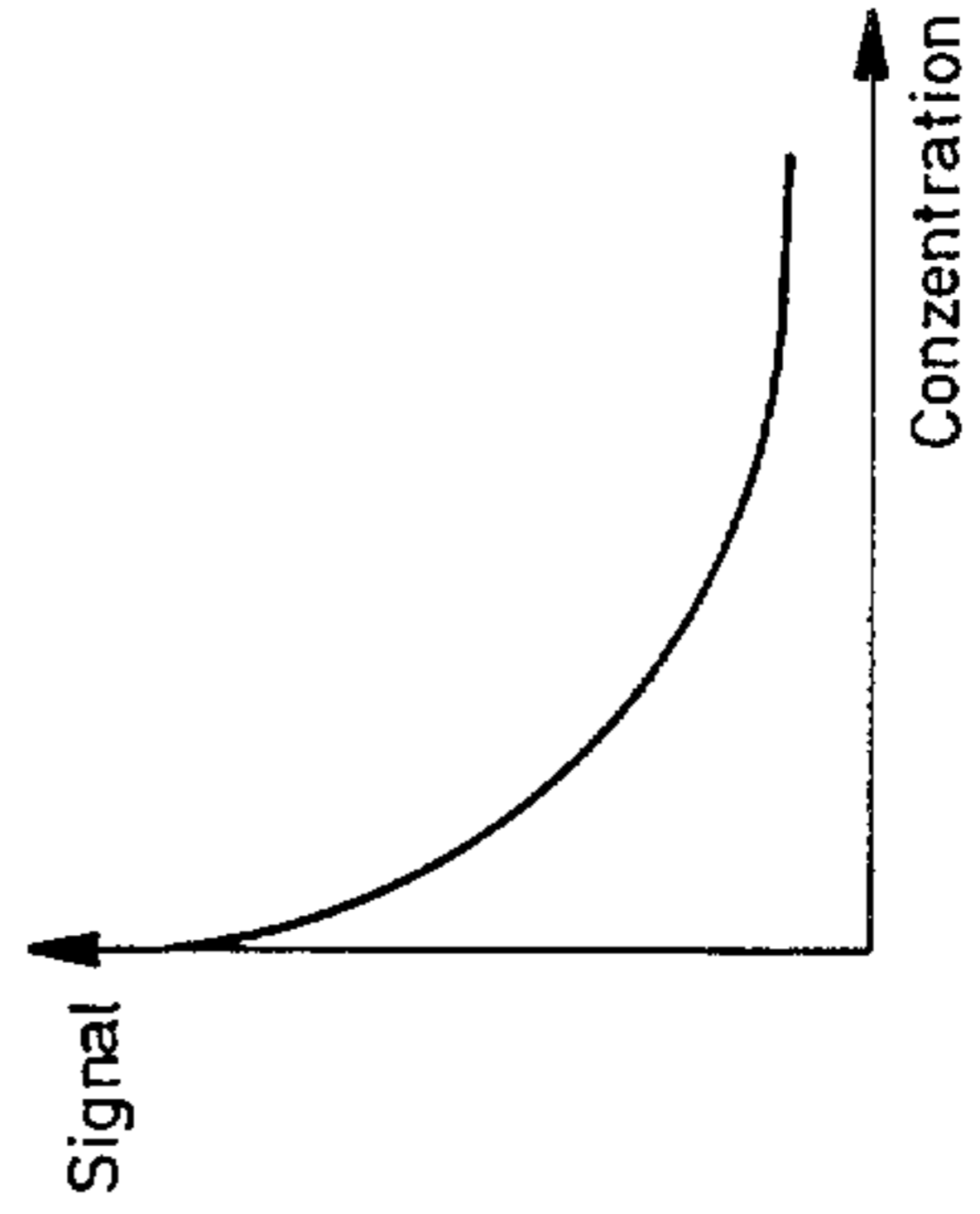


FIG. 3

Signal quench produced by anti-label antibodies

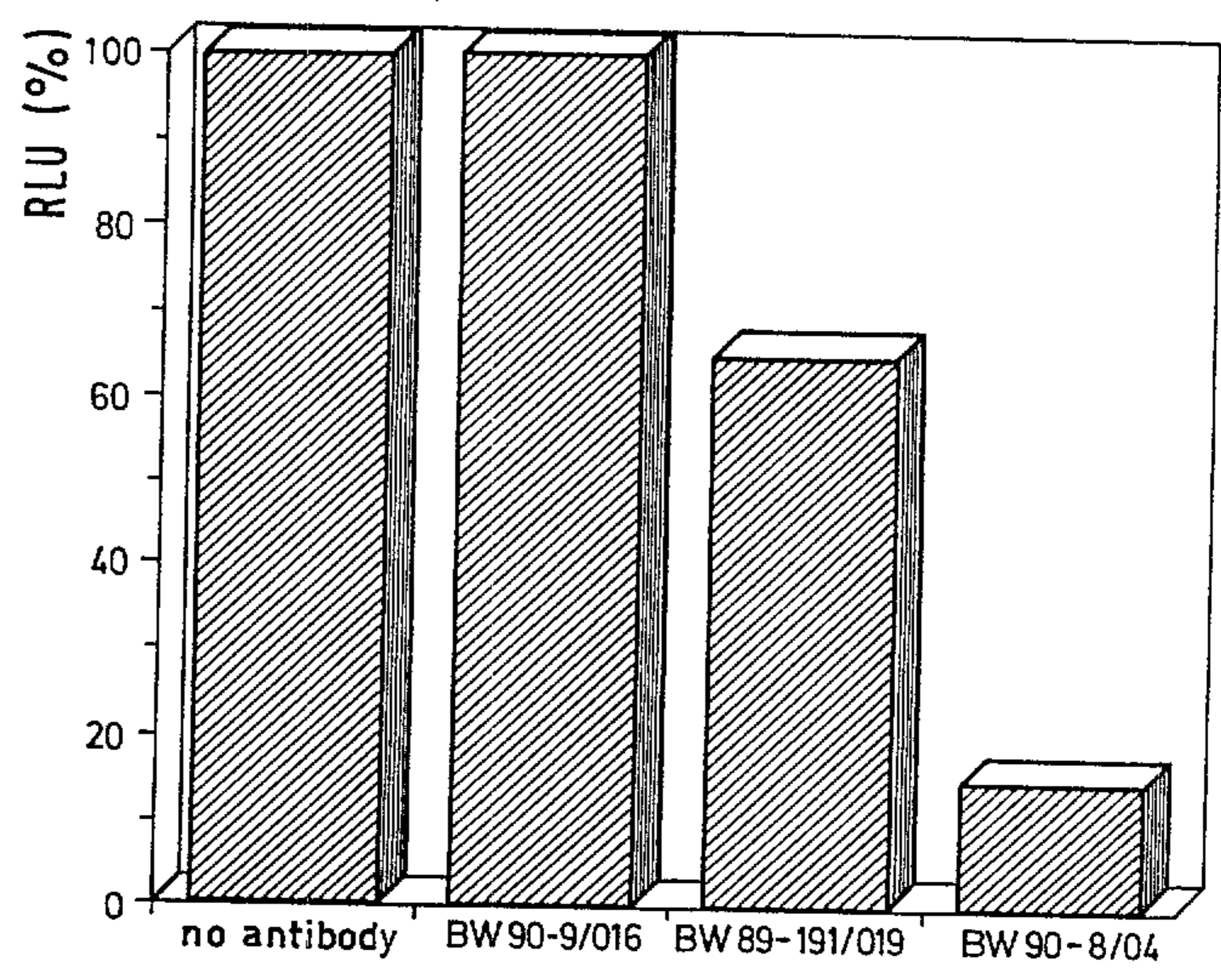


FIG. 4 Assays in a multiphase system

(3) Example: Homogeneous assays (1)

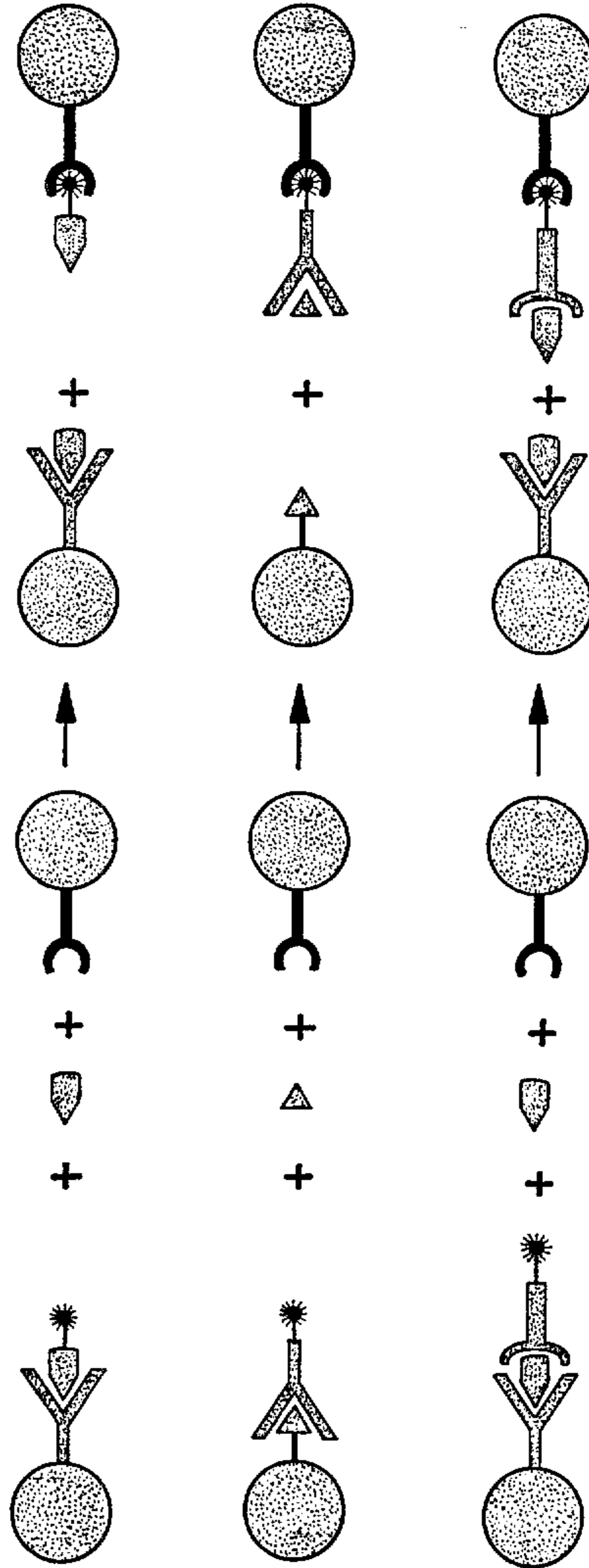


FIG. 5 Assays in a multiphase system  
(3) Example: Homogeneous assays (2)

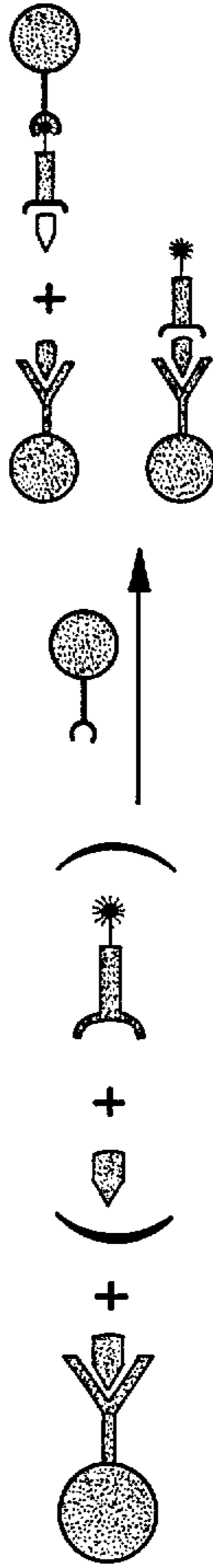
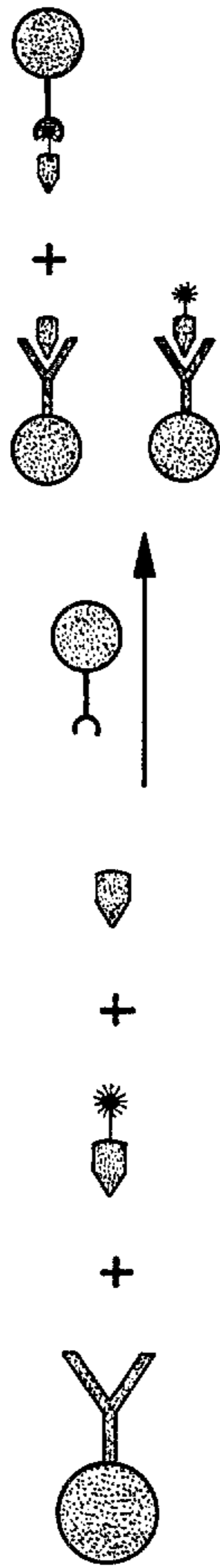


FIG. 6

Assays in a multiphase system

(3) Example: Homogeneous assays (4)

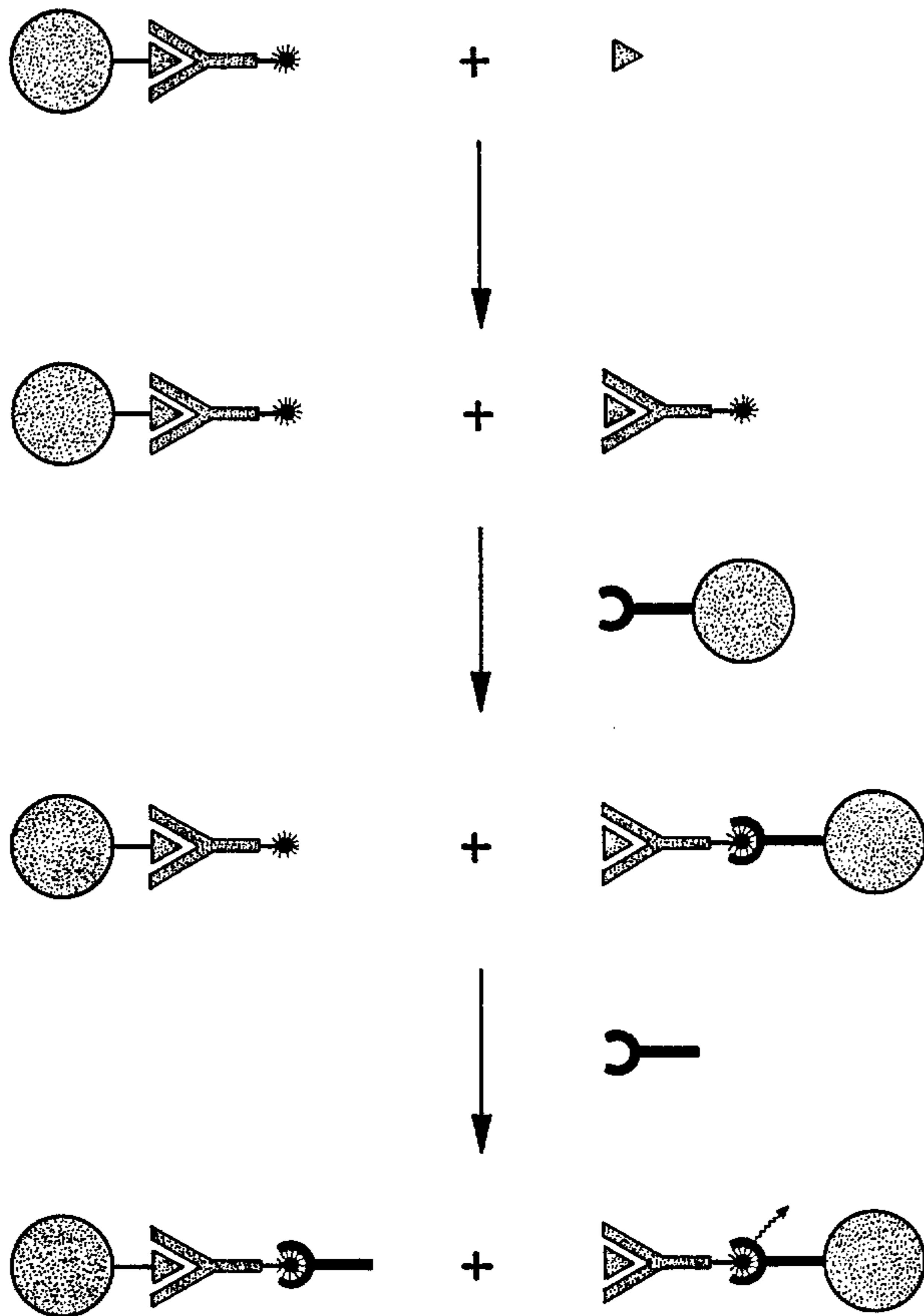


FIG. 7

Assays in a multiphase system

(3) Example: Homogenous assays (5)

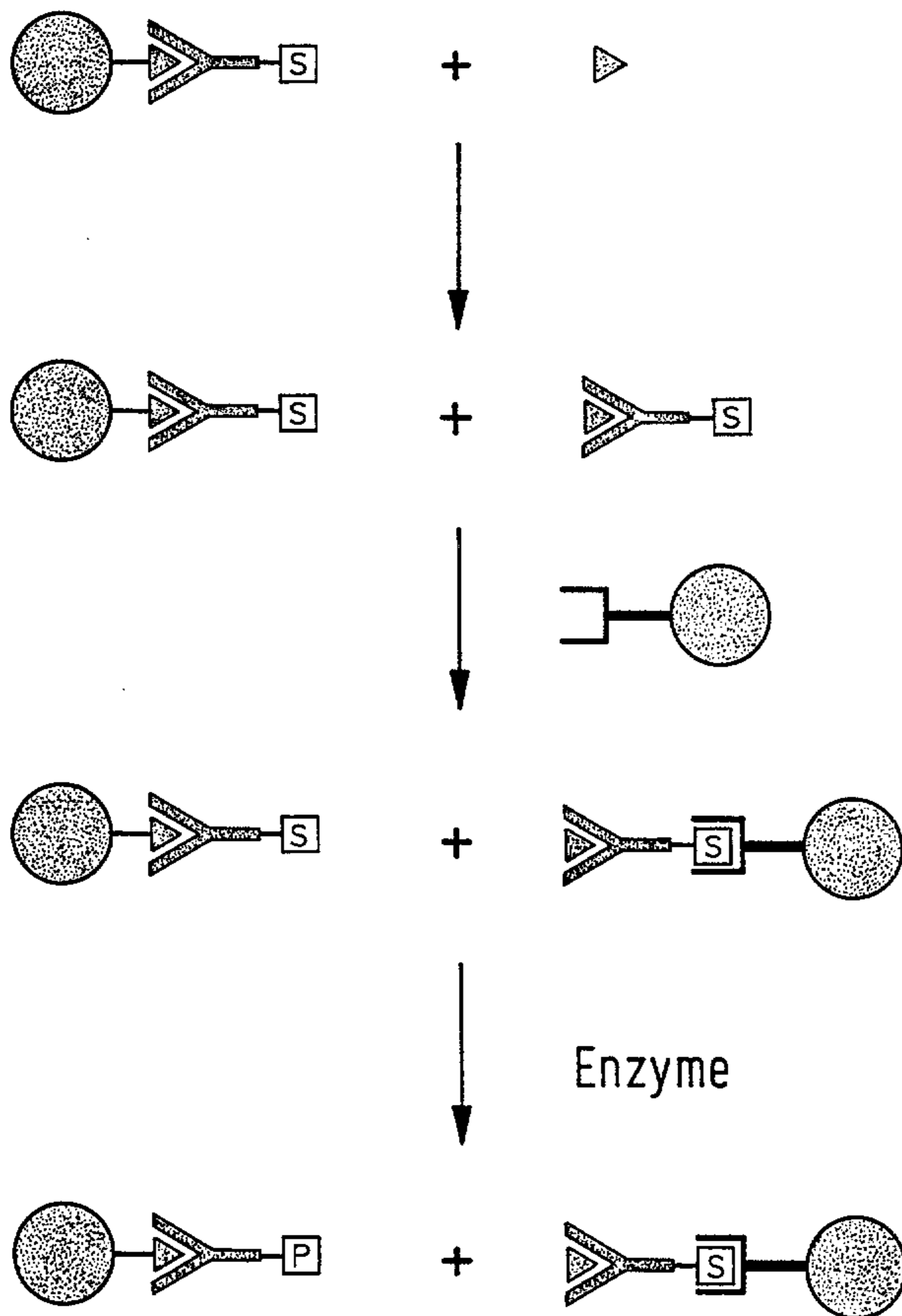
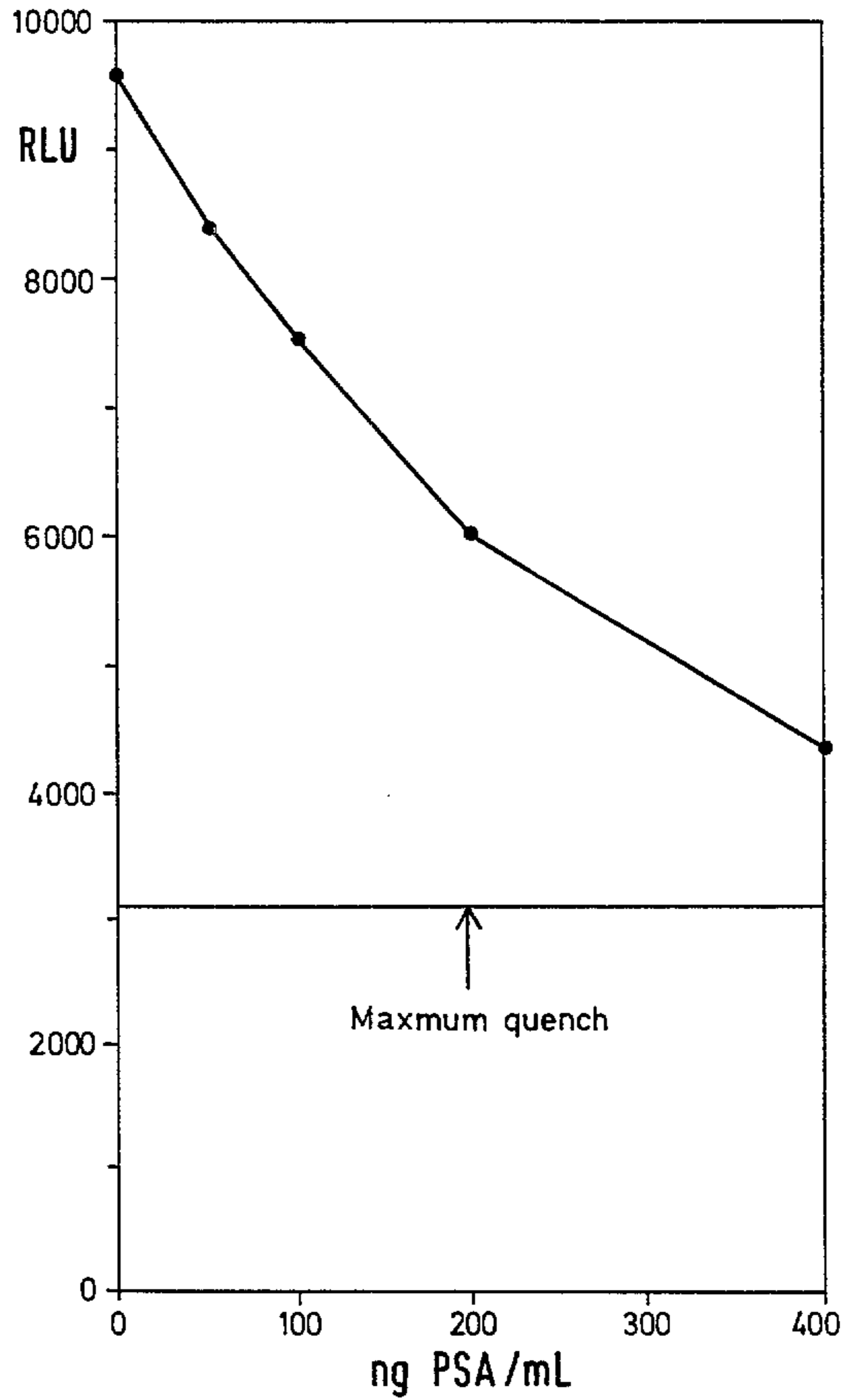


FIG. 8



Standard curve 1:  
Luminescence immunoassay (LIA) for determining PSA

FIG. 8a

Assay implementation for standard curve 1

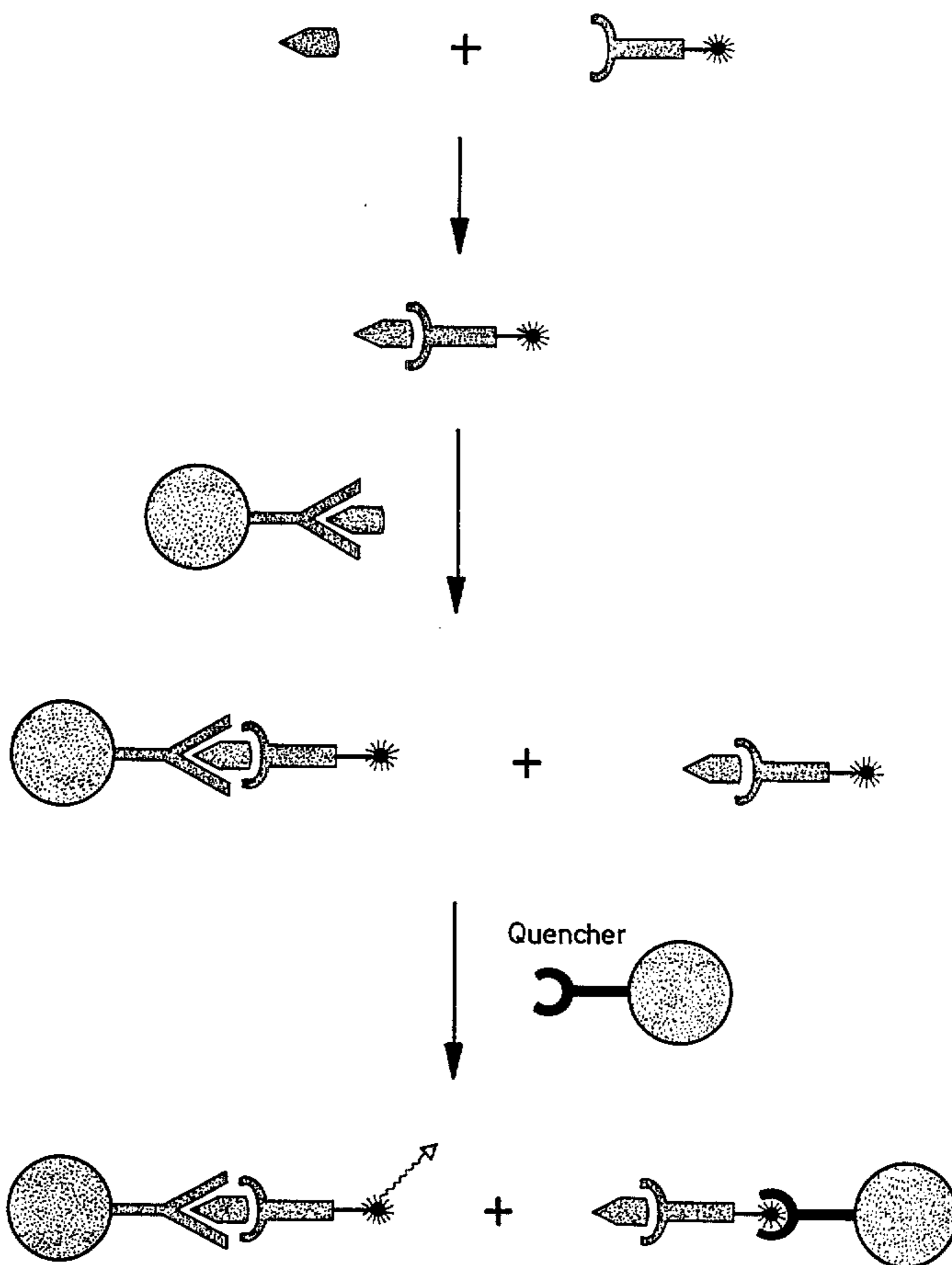
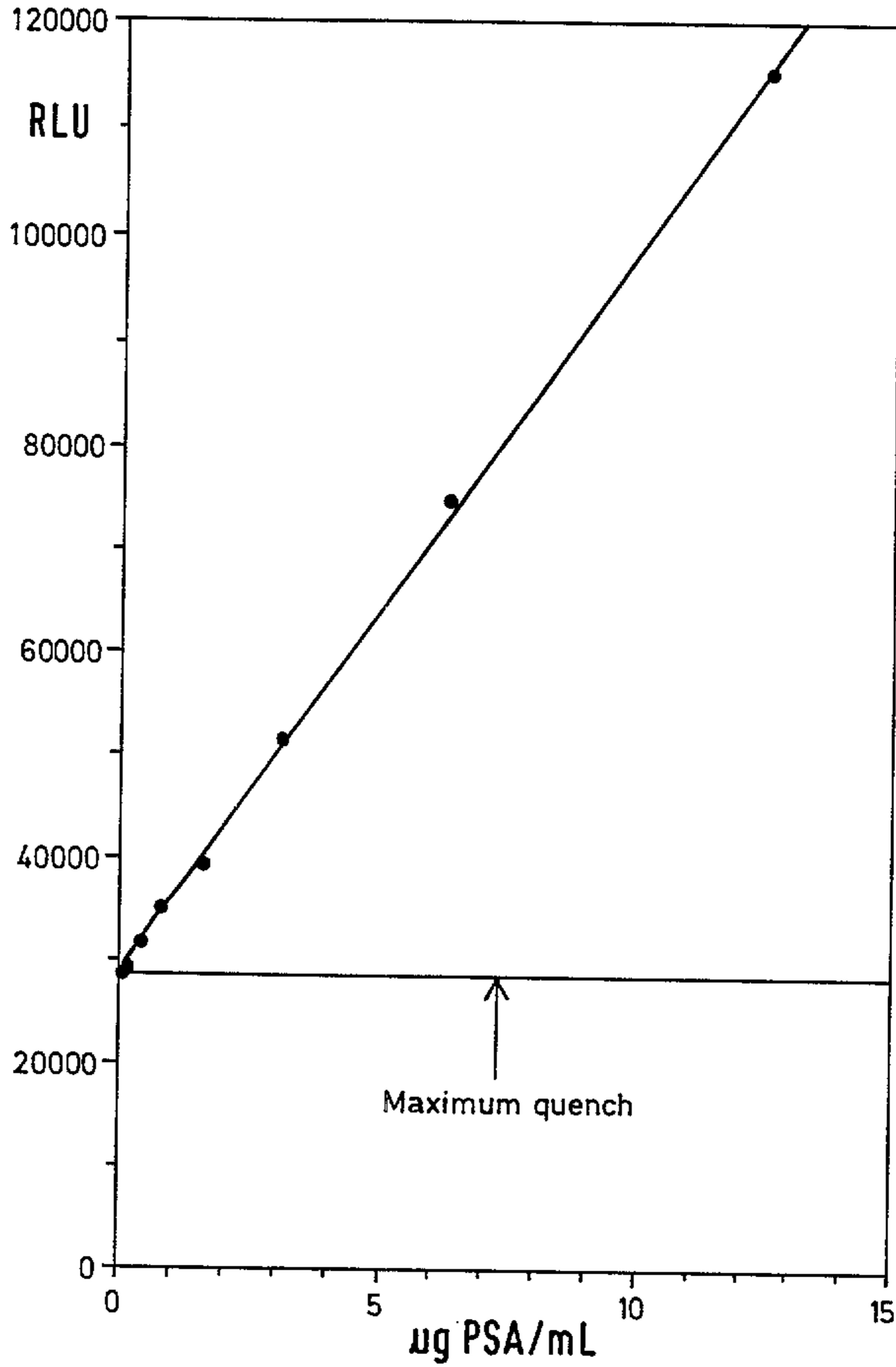


FIG. 9



Standard curve 2:  
Immunoluminometric assay (ILMA) for determining PSA

FIG.9a

Assay implementation for standart curve 2

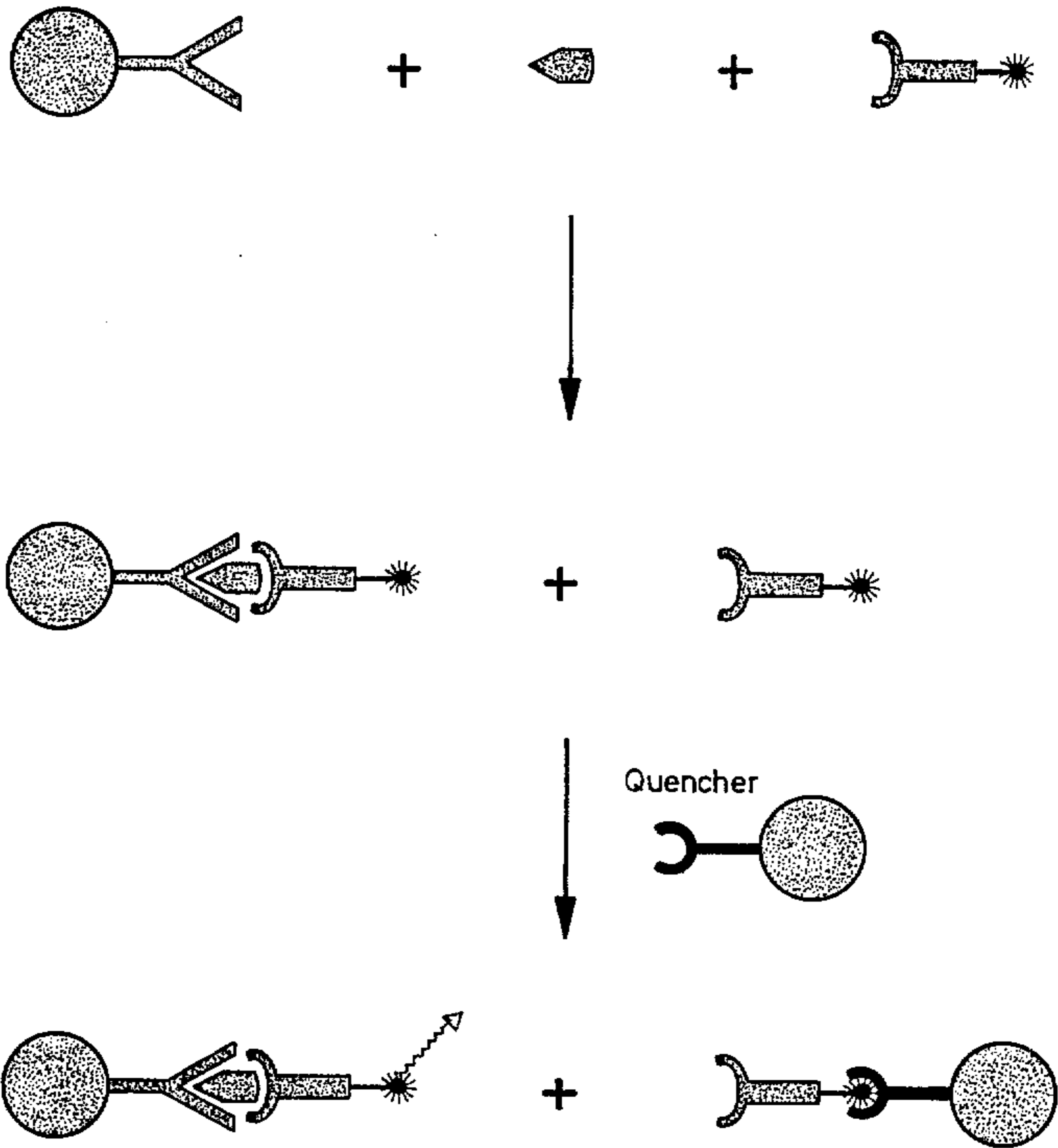
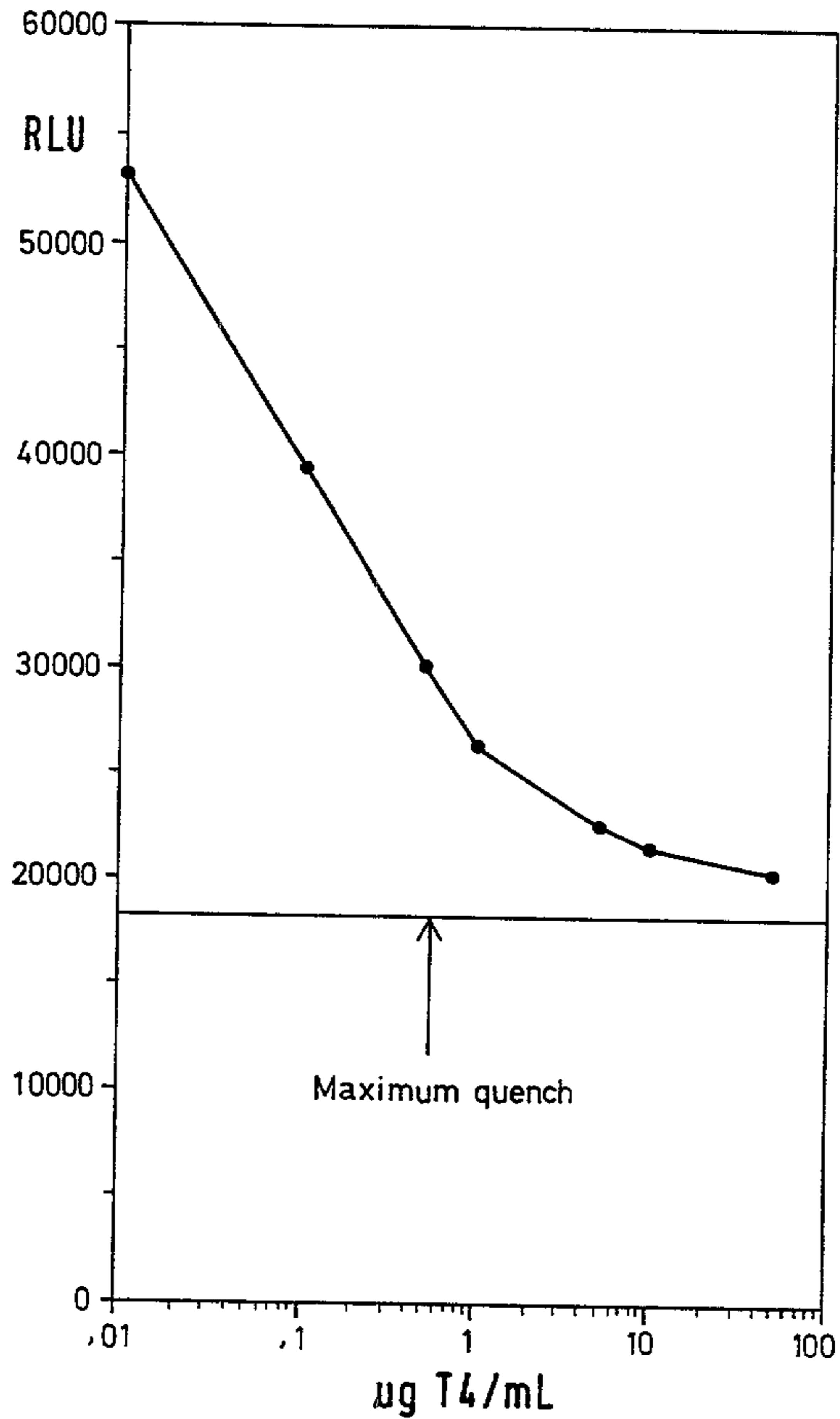


FIG. 10



Standard curve 3:  
SPALT assay for determining thyroxine

FIG. 10a

Assay implementation for standard curve 3

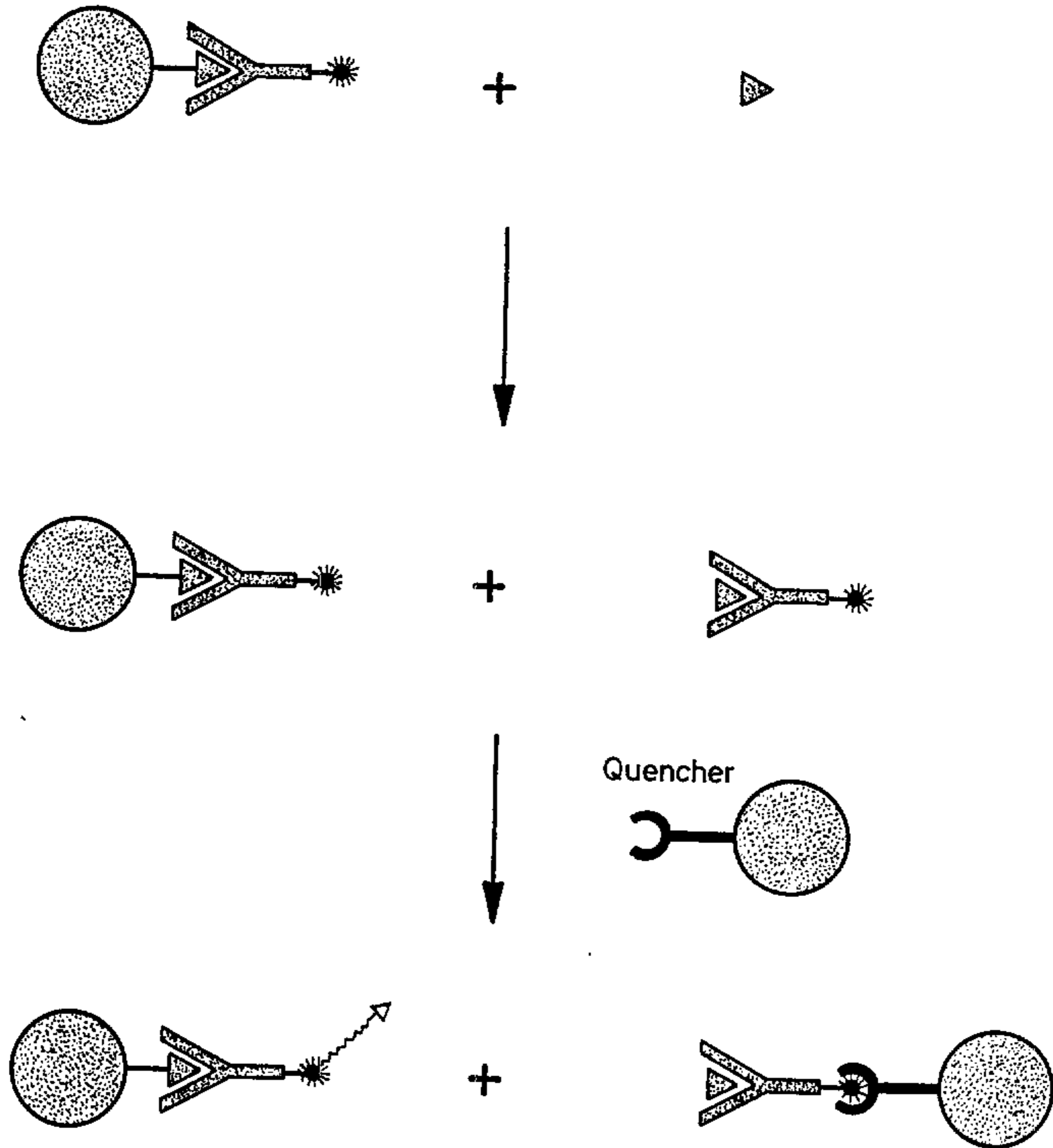
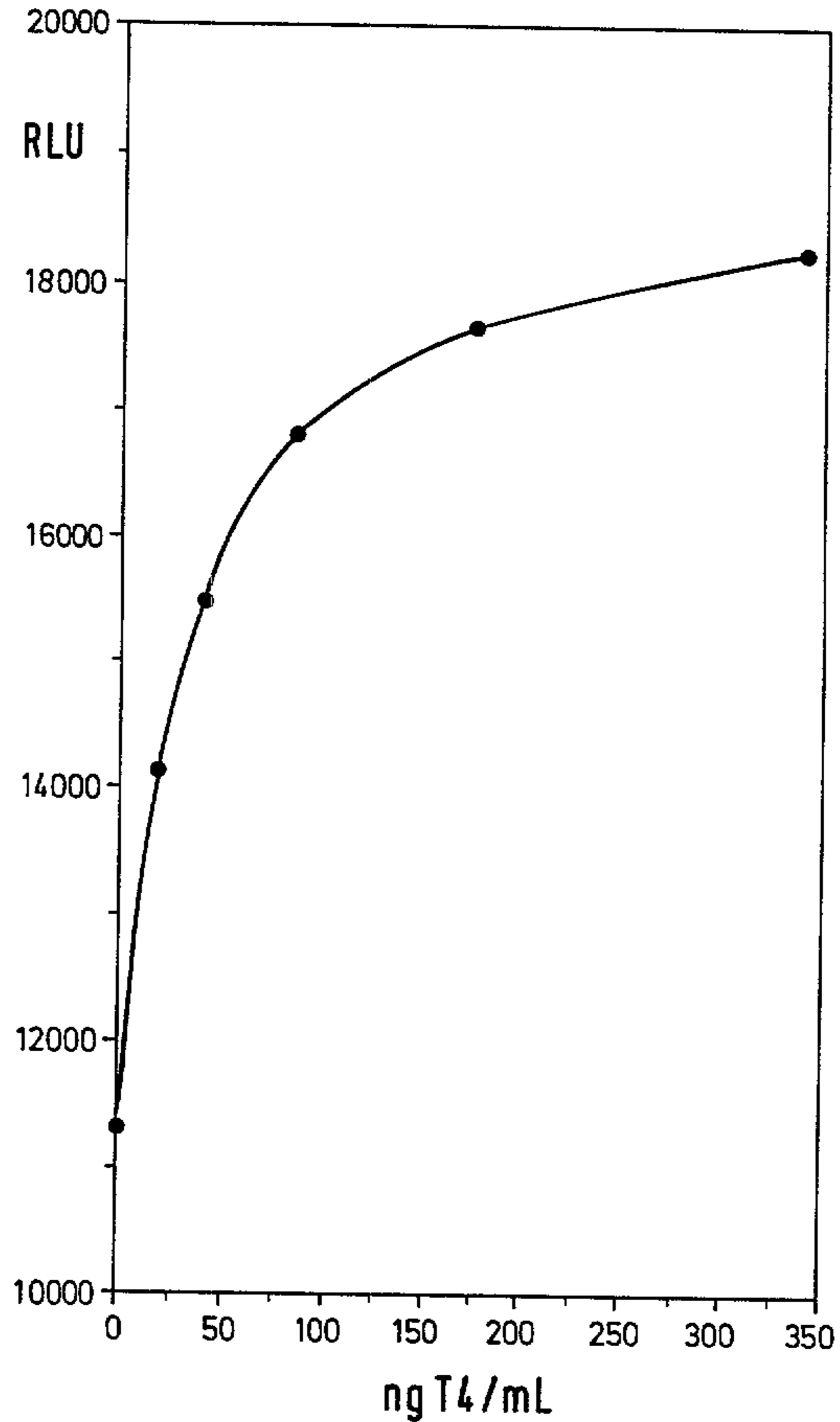


FIG.11

Standard curve 4:  
Luminescence immunoassay (LIA) for determining  
thyroxine (protector/quencher method)

FIG. 11a

Assay implementation for standard curve 4

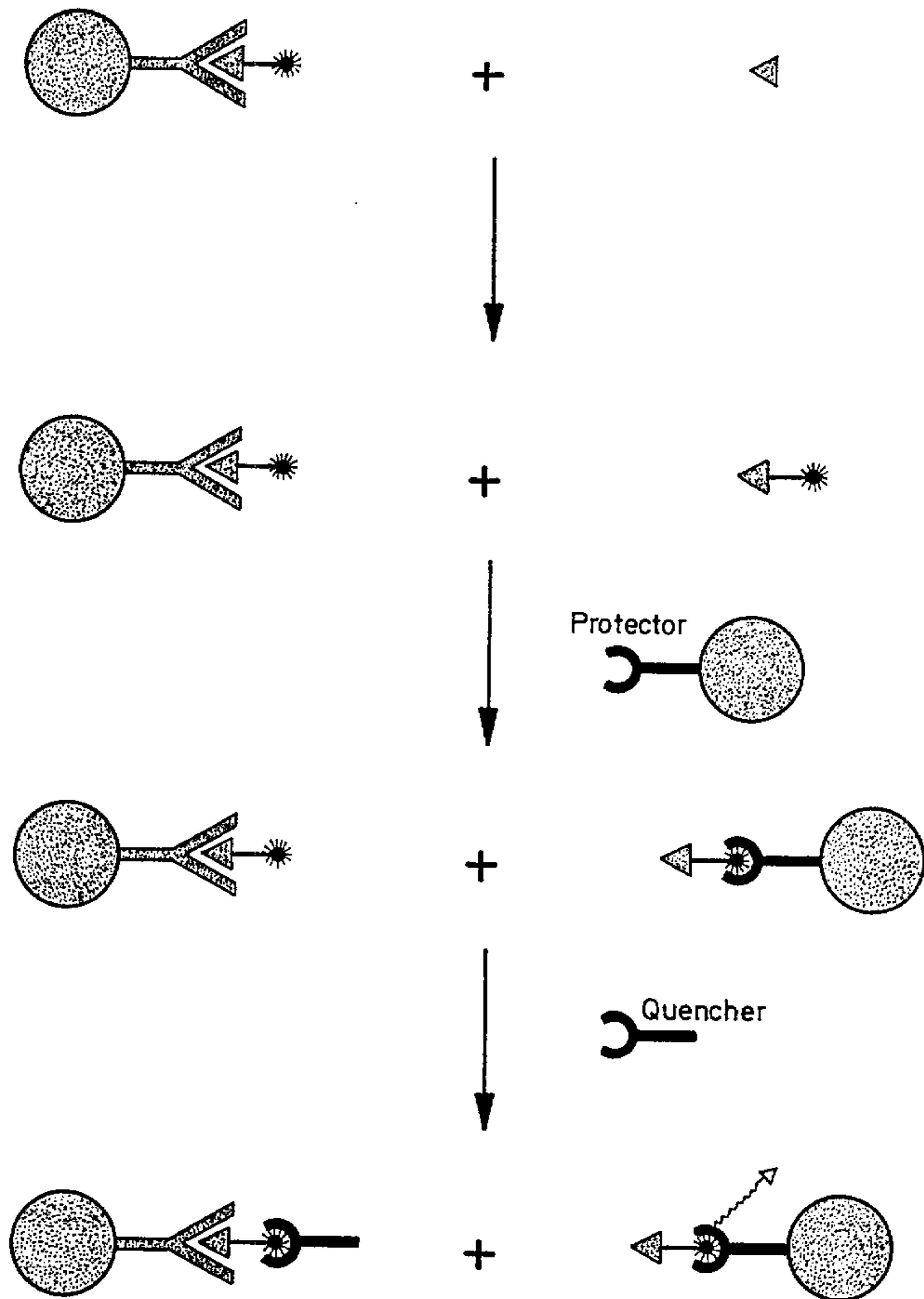
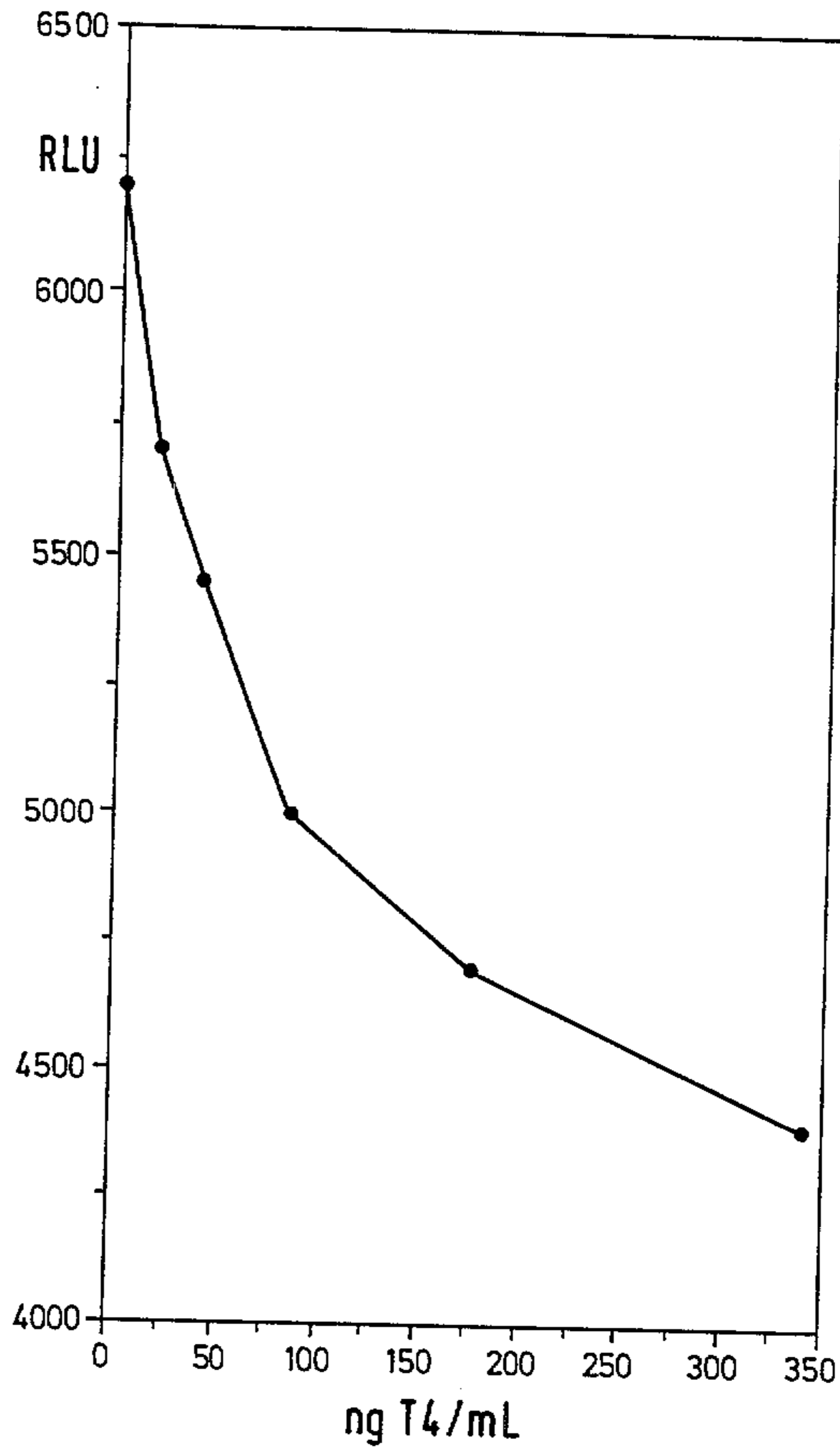


FIG.12



Standard curve 5:  
Luminescence immunoassay (LIA) for determining thyroxine

FIG.12a

Assay implementation for standard curve 5

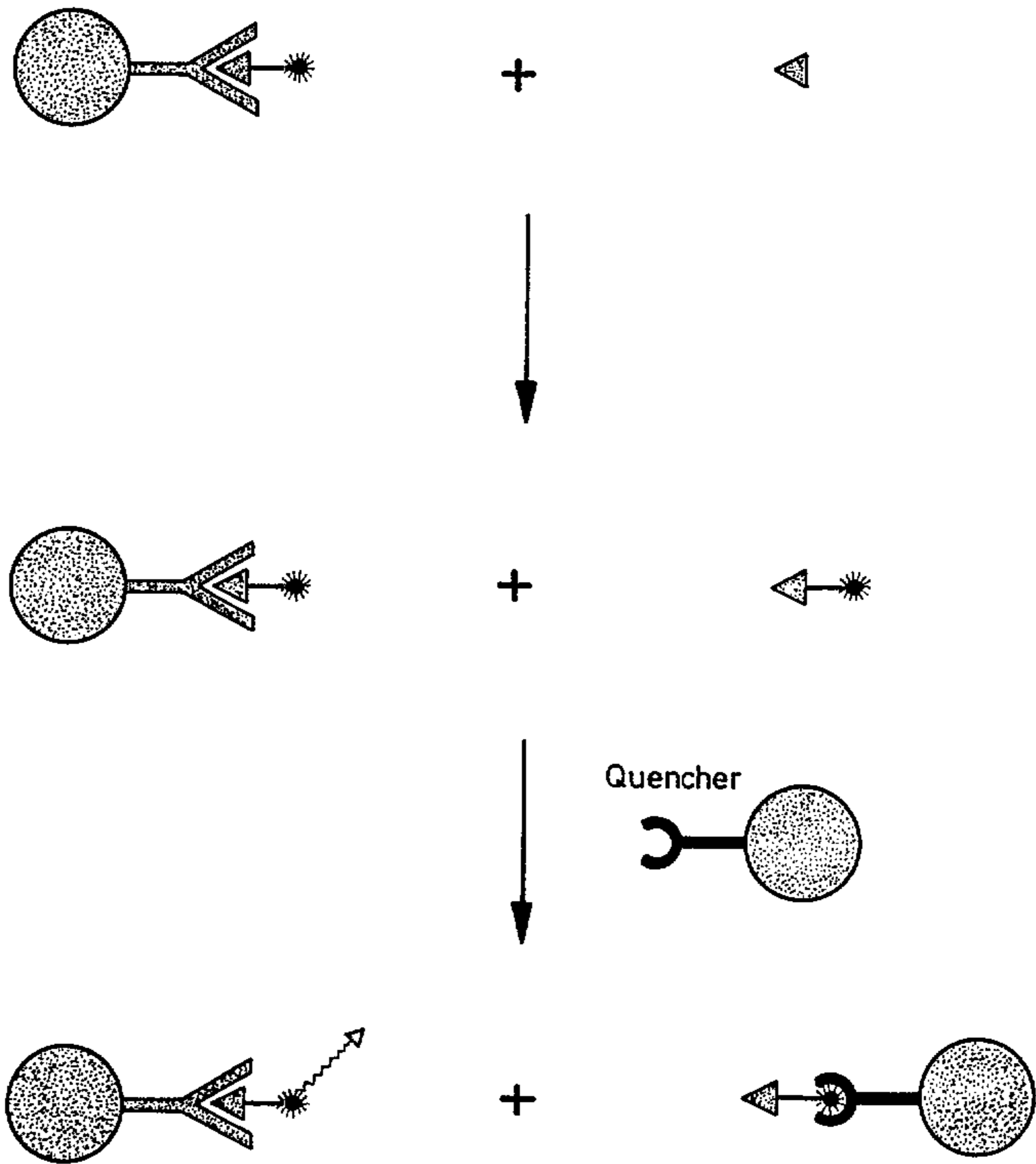
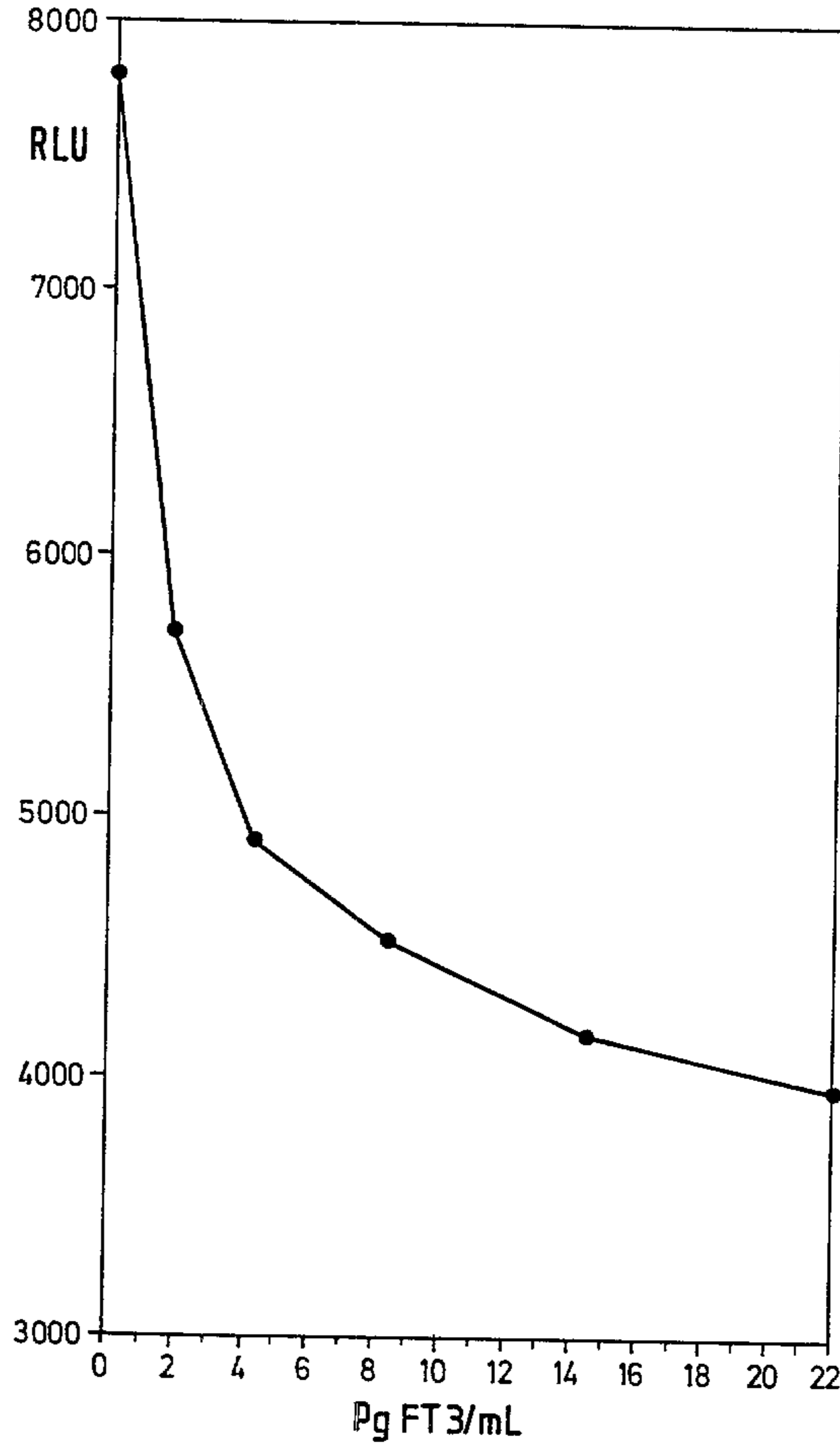


FIG. 13



Standard curve 6:  
Luminescence immunoassay (LIA) for determining FT3

FIG. 13a

Assay implementation for standard curve 6

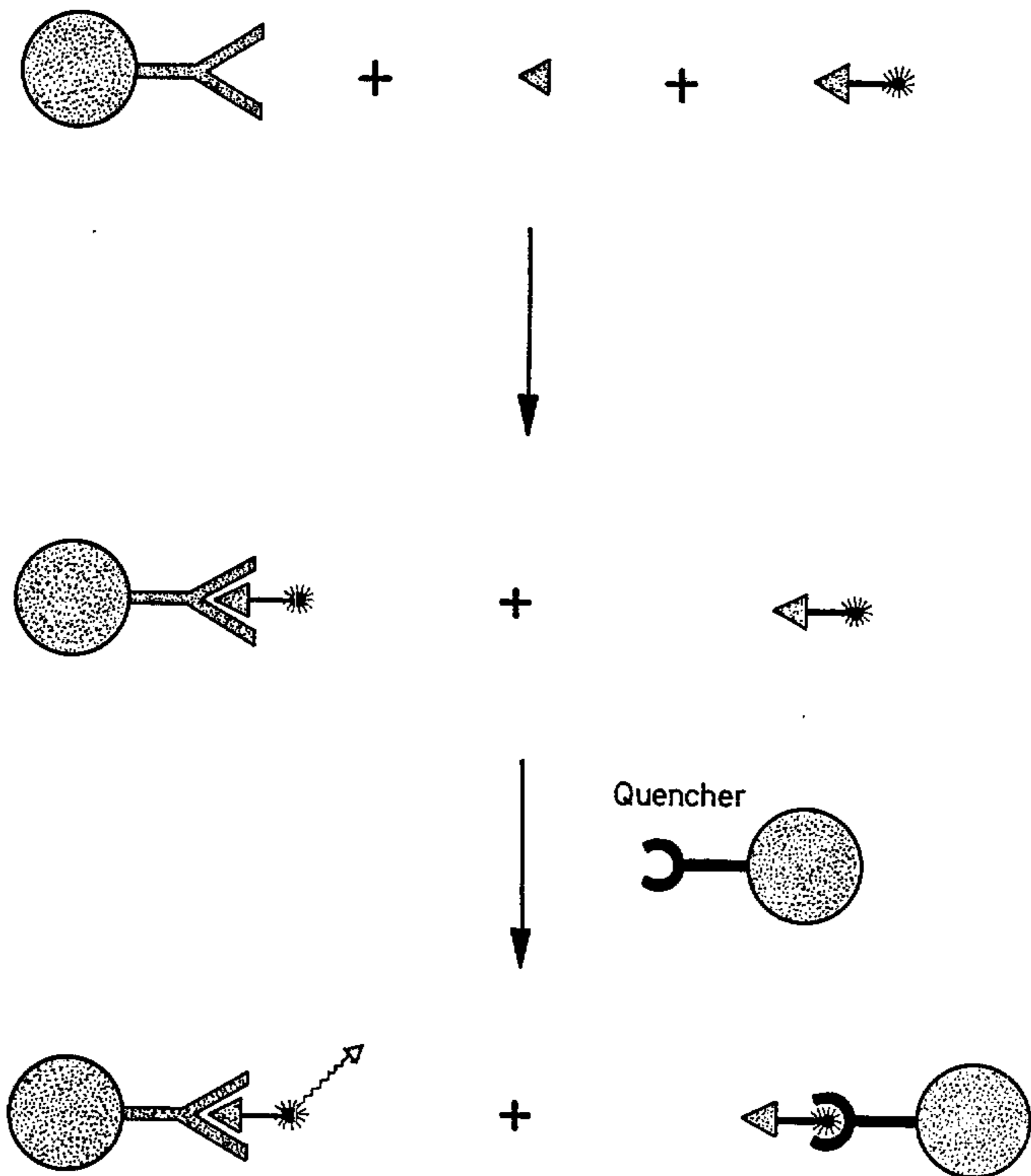
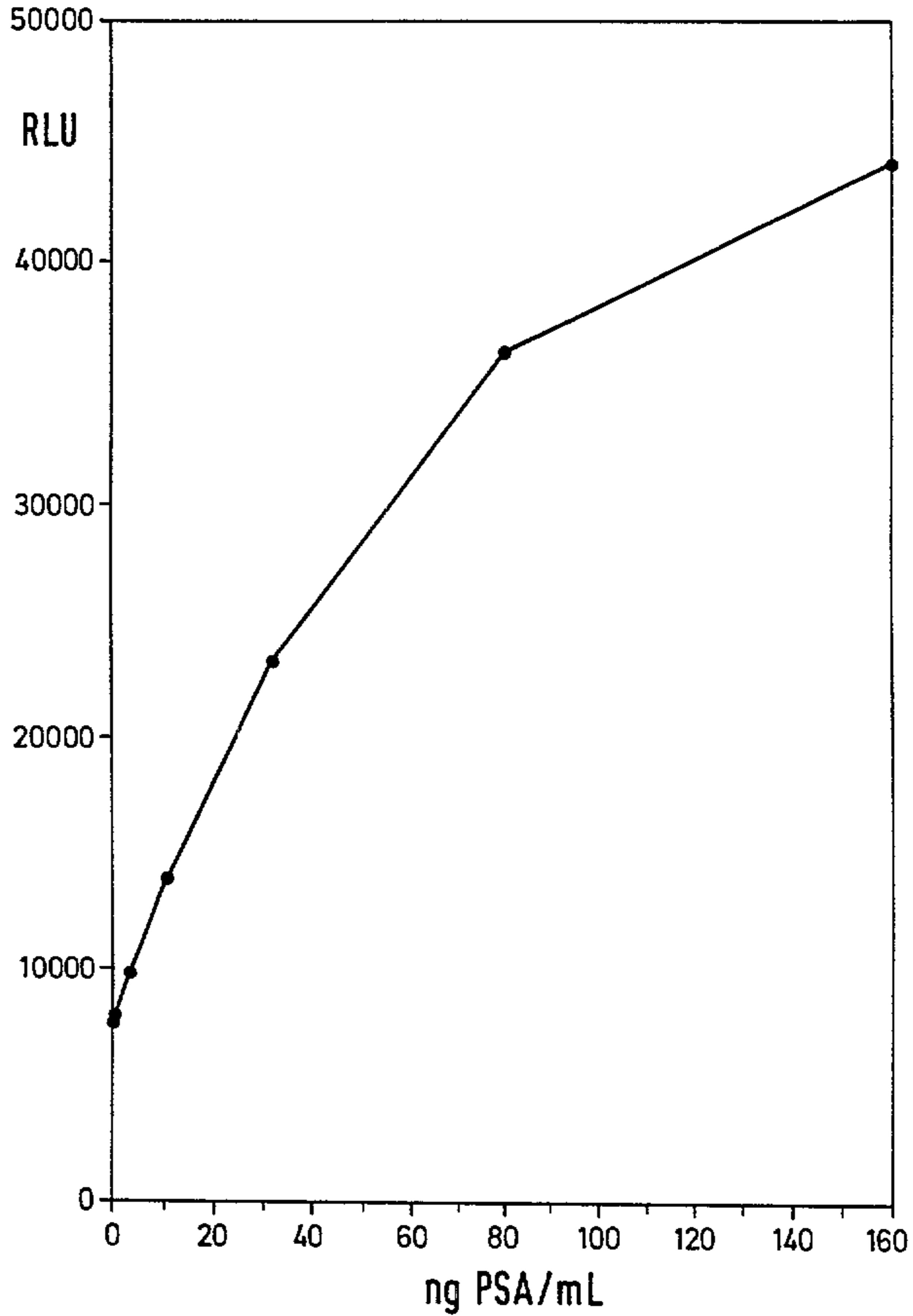
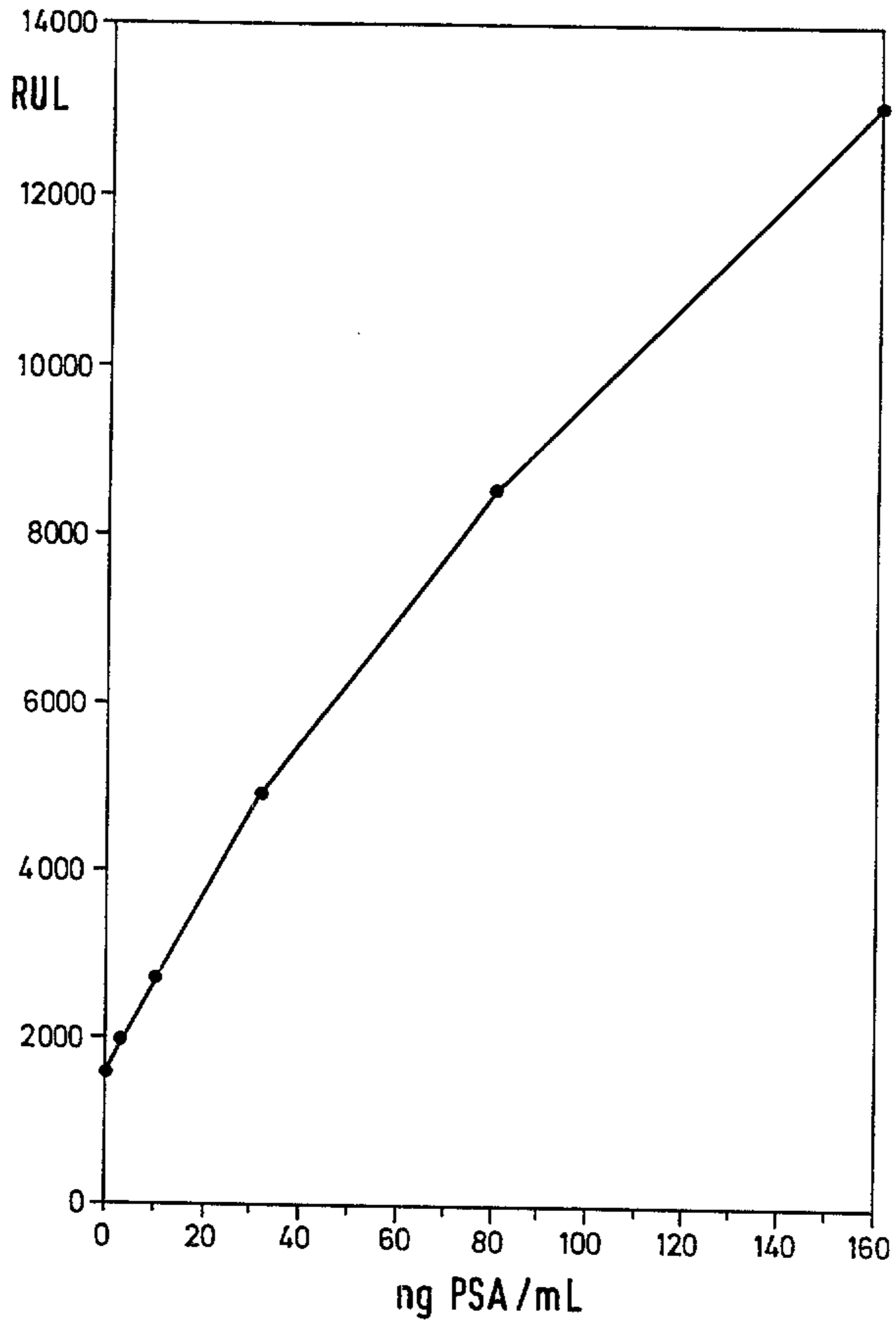


FIG. 14



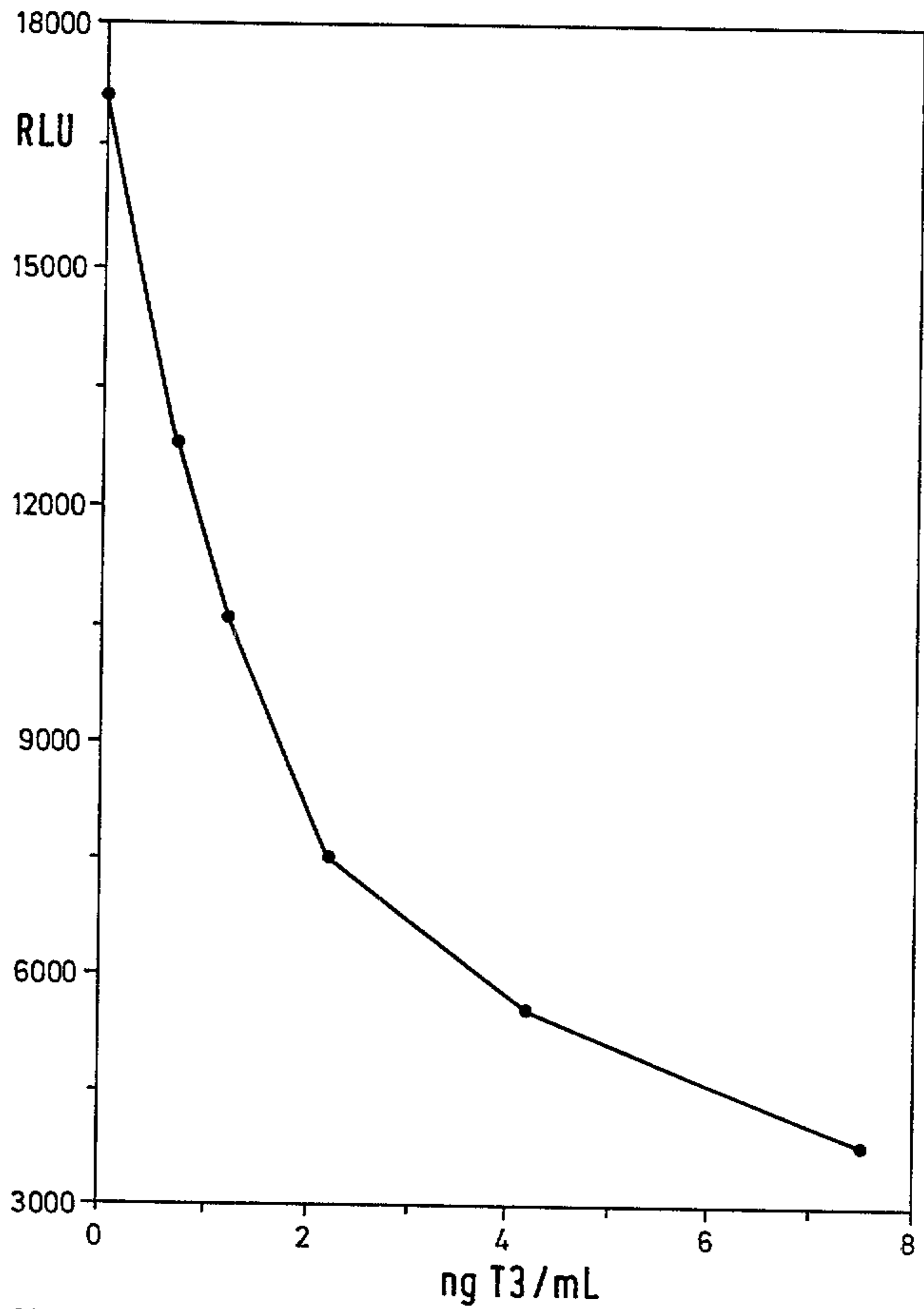
Standard curve 7:  
Immunoluminometric assay (ILMA) for determining PSA

FIG.15

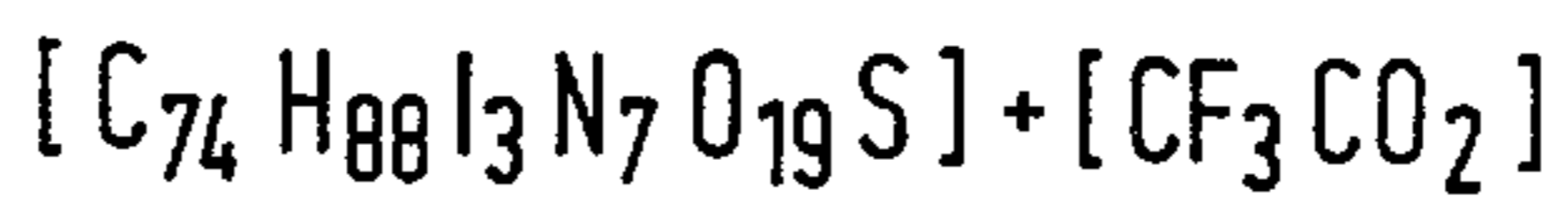
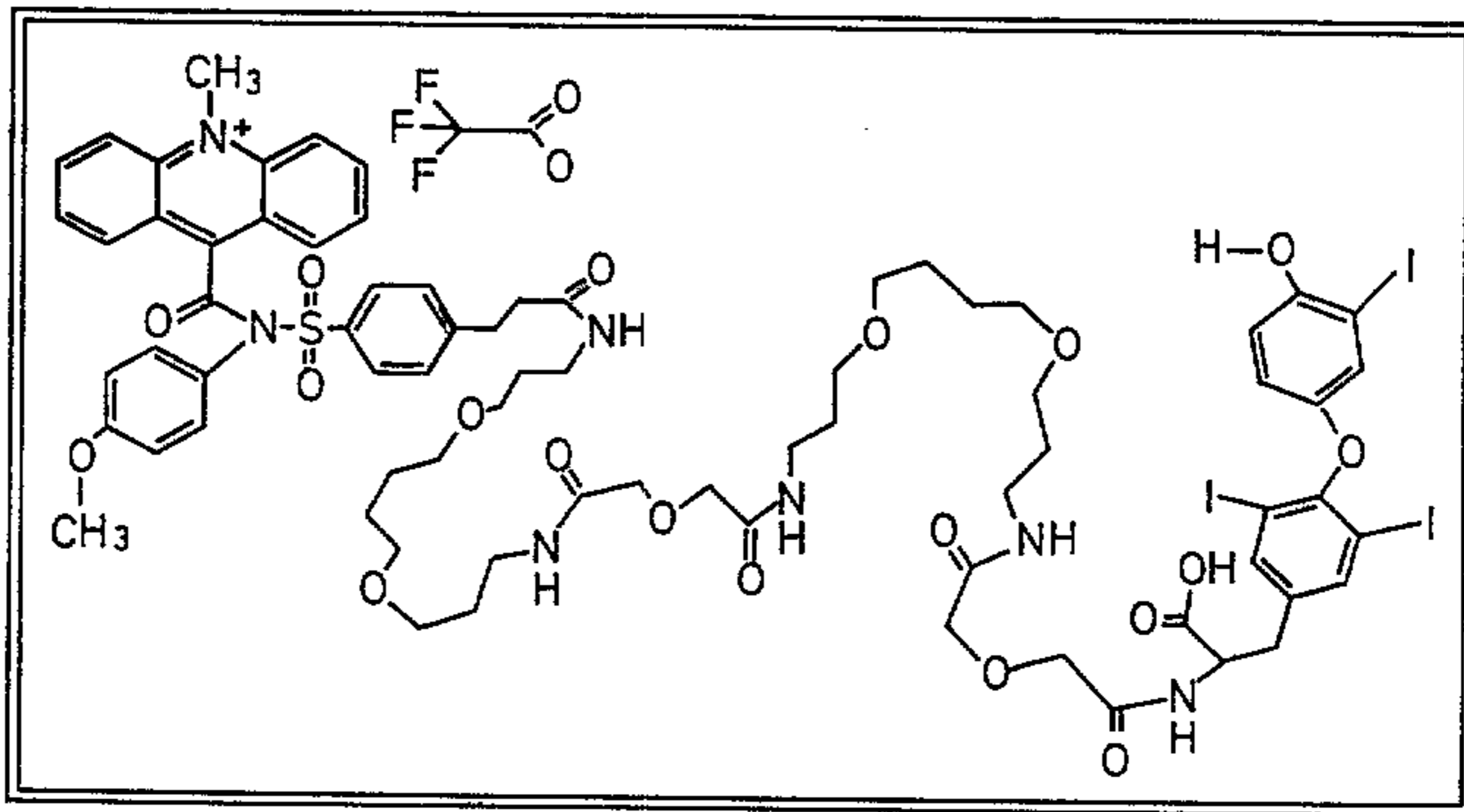


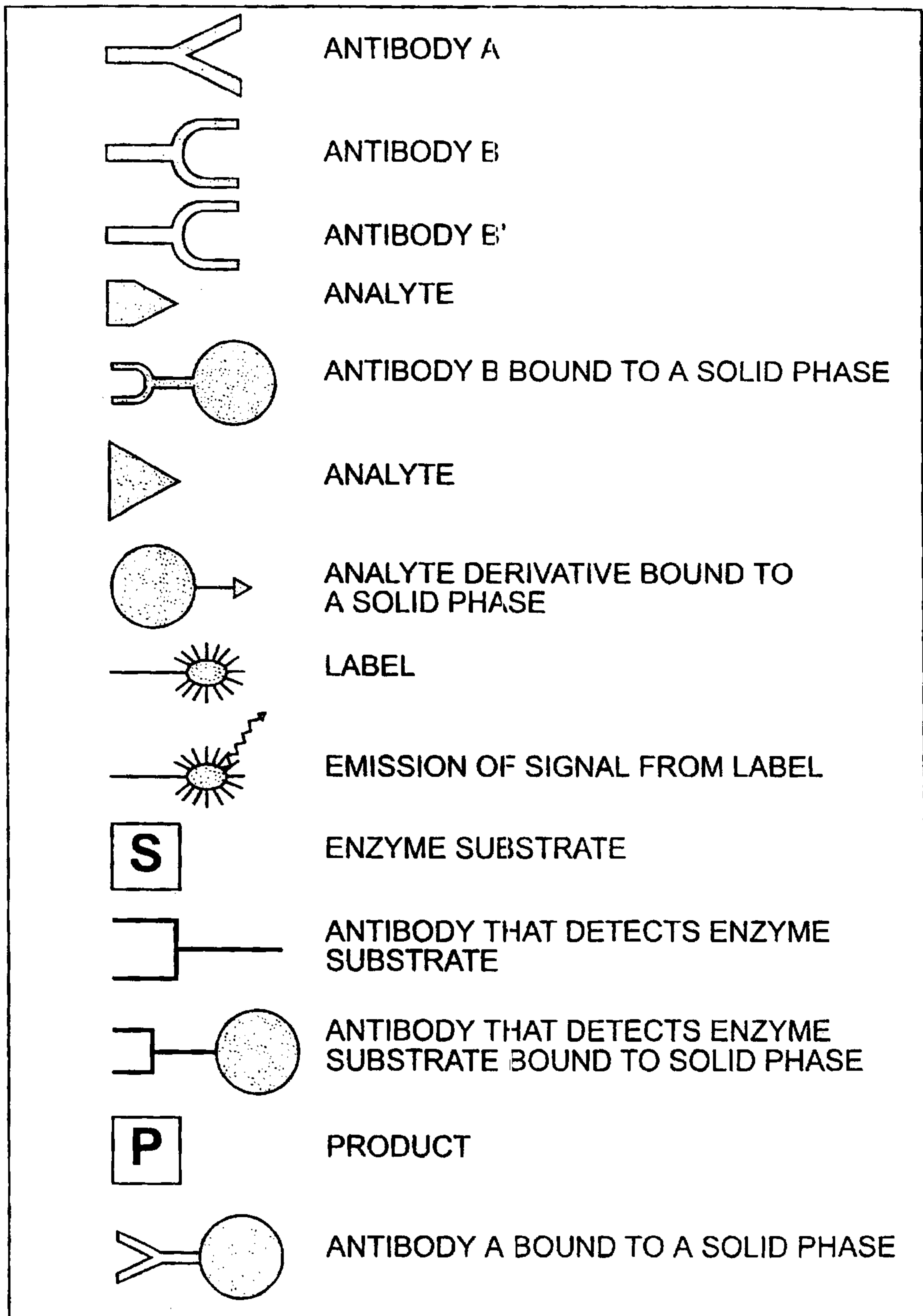
Standard curve 8:  
Immunoluminometric assay (ILMA) for determining PSA

FIG.16



Standard curve 9:  
Luminescence immunoassay (LIA) for determining T3

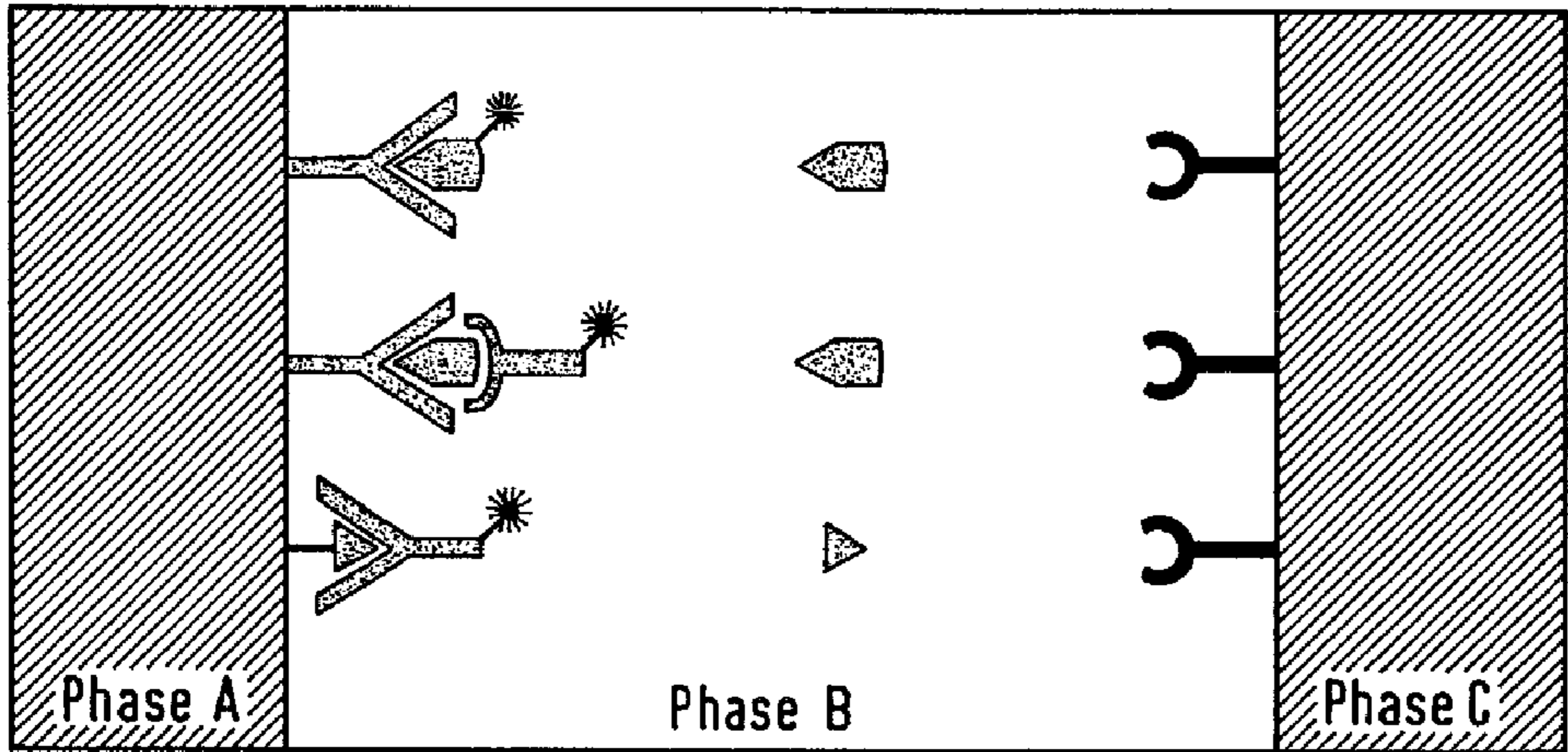
FIG. 17



**FIG. 18**

# Assays in a multiphase system

## (1) Principle



Immune reaction

- Concentration
- Equilibrium displacement
- Signal alteration
- Signal generation
- Label protection