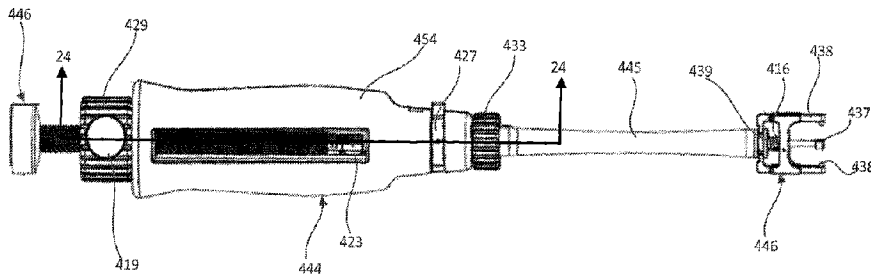




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 MITRAL VALVE



(57) **Abrégé/Abstract:**

Apparatus and methods are described herein for positioning an epicardial anchor device and measuring the load of a tether extending from a prosthetic heart valve and coupled to the epicardial anchor device. In some embodiments, an apparatus includes a handle assembly (444) coupled to an elongate member (445) and a docking member (446) coupled to a distal end of the elongate member. The docking member can be releasably coupled to an epicardial anchor device configured to secure a tether extending from a prosthetic heart valve implanted with a heart at a location on an exterior of a ventricular wall of the heart. A force sensor device (448) is coupled to the handle assembly and can measure a force exerted on the force sensor device. The force is associated with a tension of the tether extending through the elongate member and handle assembly.

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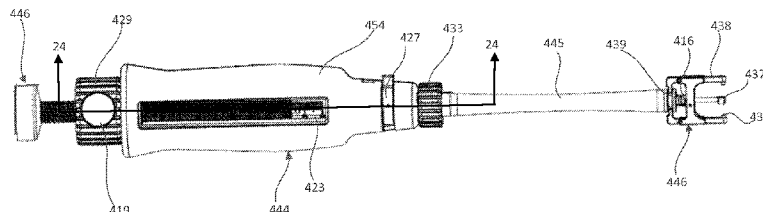
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Fig. 23

(57) Abstract: Apparatus and methods are described herein for positioning an epicardial anchor device and measuring the load of a tether extending from a prosthetic heart valve and coupled to the epicardial anchor device. In some embodiments, an apparatus includes a handle assembly (444) coupled to an elongate member (445) and a docking member (446) coupled to a distal end of the elongate member. The docking member can be releasably coupled to an epicardial anchor device configured to secure a tether extending from a prosthetic heart valve implanted with a heart at a location on an exterior of a ventricular wall of the heart. A force sensor device (448) is coupled to the handle assembly and can measure a force exerted on the force sensor device. The force is associated with a tension of the tether extending through the elongate member and handle assembly.



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**DEVICES AND METHODS FOR POSITIONING AND MONITORING TETHER
LOAD FOR PROSTHETIC MITRAL VALVE**

[1001] Σ

Background

[1002] Embodiments are described herein that relate to devices and methods for anchoring a medical device such as a prosthetic heart valve replacement, and more particularly to devices and methods for the post-deployment adjustment and/or re-positioning of such a medical device.

[1003] Some known prosthetic heart valves, such as prosthetic mitral valves, include one or more tethers that extend from the valve to the exterior of the heart, and are secured to an outer ventricular wall of the heart with an epicardial anchor device. During such procedures, positioning the anchor device and providing a desired tension to the securing tether can be challenging. Many known devices do not have the ability to make adjustments to the anchor device or to the tension of the tether after initial placement. Further, known devices do not have the ability to measure and monitor the tension on the tether during deployment of the valve to assist in providing an optimal tension and position.

[1004] Some problems associated with improper tensioning of a securing tether can include, for example, the tether becoming progressively slack over time, a tether which has been overtightened and is deforming the positioning of the deployed valve, and a tether which has been deployed in a less than optimal angular configuration or has migrated such that the valve axis is no longer orthogonal to the plane of the native valve's annulus.

[1005] Accordingly, there is a need for devices and methods for adjusting and/or repositioning a prosthetic heart valve after its initial deployment and for monitoring the tension on a securing tether extending from the prosthetic heart valve.

Summary

[1006] Apparatus and methods are described herein for positioning an epicardial anchor device and measuring the load of a tether extending from a prosthetic heart valve and coupled to the epicardial anchor device. In some embodiments, an apparatus includes a handle assembly coupled to an elongate member and a docking member coupled to a distal end of the elongate member. The docking member can be releasably coupled to an epicardial anchor device configured to secure a tether extending from a prosthetic heart valve implanted with a heart at a location on an exterior of a ventricular wall of the heart. A force sensor device is coupled to the handle assembly and can measure a force exerted on the force sensor device. The force is associated with a tension of the tether extending through the elongate member, handle assembly and force sensor device.

Brief Description of the Drawings

[1007] FIG. 1 is a schematic cross-sectional illustration of portion of a heart with a prosthetic mitral valve implanted therein and an epicardial anchor device anchoring the mitral valve in position.

[1008] FIG. 2 is a schematic illustration of an epicardial anchor device, according to an embodiment.

[1009] FIG. 3 is a schematic illustration of a positioning device, according to an embodiment.

[1010] FIG. 4 is a top perspective view of an epicardial anchor device, according to another embodiment.

[1011] FIG. 5 is a top view of the epicardial anchor device of FIG. 4.

[1012] FIG. 6 is an exploded view of the epicardial anchor device of FIG. 4.

[1013] FIG. 7 is a cross-sectional perspective view of the epicardial anchor device of FIG. 4 with a locking pin of the device shown in a first position.

[1014] FIG. 8 is a cross-sectional side view of the epicardial anchor device of FIG. 4 with the locking pin of the device shown in the first position.

[1015] FIG. 9 is a cross-sectional bottom perspective view of the epicardial anchor device of FIG. 4 with the locking pin shown in a second position.

[1016] FIGS. 10 and 11 are a top perspective and a bottom perspective view, respectively, of a hub member of the epicardial anchor device of FIG. 4.

[1017] FIG. 12 is an enlarged top view of a portion of the epicardial anchor device of FIG. 4.

[1018] FIG. 13 is a perspective view of a positioning device, according to an embodiment.

[1019] FIG. 14 is a top view of a portion of the positioning device of FIG. 13.

[1020] FIG. 15 is a cross-sectional view of the portion of the positioning device of FIG. 14.

[1021] FIG. 16A is a perspective view and FIG. 16B is a top view of a portion of the positioning device of FIG. 13.

[1022] FIG. 17A is a perspective view of a portion of the positioning device of FIG. 13 shown partially exploded.

[1023] FIG. 17B is a perspective view of the portion of the positioning device of FIG. 17A.

[1024] FIG. 18 is a top view of a positioning device, according to another embodiment.

[1025] FIG. 19 is a perspective view of a portion of the positioning device of FIG. 18 shown partially exploded.

[1026] FIG. 20 is a perspective view of the portion of the positioning device of FIG. 19.

[1027] FIG. 21 is a schematic illustration of a portion of the positioning device of FIG. 18.

[1028] FIG. 22 is a perspective view of a positioning device, according to another embodiment, shown coupled to an epicardial anchor device.

[1029] FIG. 23 is a top view of the positioning device of FIG. 22.

[1030] FIG. 24 is a cross-sectional view of a portion of the positioning device of FIG. 22, taken along line 24-24 in FIG. 23.

[1031] FIG. 25 is a perspective view of a portion of the positioning device of FIG. 22.

[1032] FIG. 26 is a perspective view of a force sensor device of the positioning device of FIG. 22.

[1033] FIG. 27 is an exploded perspective view of the force sensor device of FIG. 26.

[1034] FIG. 28 is a perspective view of a portion of the force sensor device of FIG. 26.

[1035] FIG. 29 is a perspective view of a portion of the positioning device of FIG. 22.

[1036] FIG. 30 is a side view of the positioning device of FIG. 22.

[1037] FIG. 31 is a partial cross-sectional side view of a tension limiting device according to an embodiment.

[1038] FIG. 32 is a top view of a tether release tool, according to an embodiment.

[1039] FIG. 33 is a perspective view of an end portion of the tether release tool of FIG. 32.

[1040] FIG. 34 is a perspective view of a portion of the tether release tool of FIG. 32 shown being coupled to an epicardial anchor device.

[1041] FIG. 35 is a perspective view of a portion of the tether release tool of FIG. 32 shown coupled to the epicardial anchor device of FIG. 34.

[1042] FIG. 36 is a perspective view of a force sensor device according to an embodiment.

[1043] FIG. 37 is an exploded perspective view of the force sensor device of FIG. 36.

[1044] FIG. 38 is a cross-sectional perspective view of the force sensor device of FIG. 36.

[1045] FIG. 39 is a side view of a portion of a tether with a marker band according to an embodiment.

Detailed Description

[1046] Apparatus and methods are described herein that can be used for the post-deployment adjustment and/or re-positioning of a transcatheter prosthetic heart valve, such as a mitral valve, that has been deployed into the annulus of a native valve, such as a mitral valve. For example, such a prosthetic mitral valve can be anatomically secured in a two-phase process that includes securing the prosthetic mitral valve in the native annulus using a atrial cuff and a tether axial tensioning system in combination with a laterally expanded stent, and to methods for making such systems.

[1047] In some embodiments, apparatus and methods are described herein for monitoring the tension applied to a securing tether extending from a prosthetic mitral valve that has been deployed into the native mitral valve.

[1048] Various embodiments described herein address problems concerning valve delivery and deployment, valve compliance, perivalvular leaking, hemodynamic issues such as left ventricular outflow tract (LVOT) interference, clotting, cardiac remodeling, etc.

[1049] In some embodiments, an adjustable tether and epicardial anchor device for a compressible prosthetic heart valve replacement are described herein, which can be deployed into a closed beating heart using, for example, a transcatheter delivery system. In some embodiments, such a valve replacement device can be deployed in a minimally invasive fashion and by way of example considers a minimally invasive surgical procedure utilizing the intercostal or sub-xiphoid space for valve introduction. To accomplish this, the valve is formed so that it can be compressed to fit within a delivery system and then ejected from the delivery system into the target location, for example, the annulus of the mitral or tricuspid valve.

[1050] In some embodiments, there is provided a method of adjusting the length and/or tension of a tether for a tethered transcatheter prosthetic heart valve after a transcatheter valve implantation procedure in a patient. Such a method can include adjusting the transluminal length of a ventricular tether, wherein the tether is anchored between an epicardial anchor device that is releasably affixed to an external epicardial surface of the heart and a valve-based fastening system on a transcatheter prosthetic heart valve that is deployed in the native valve annulus of the patient. Upon releasing the tether from the epicardial anchor device, the

tether length and/or tension is adjusted and the tether is re-fastened to the epicardial anchor device.

[1051] In another embodiment, there is provided a method as above, further including capturing the tether, threading the tether through a tether release tool, re-engaging the tether release tool with the epicardial anchor device, unlocking the pin and releasing the tether. In some embodiments, after adjusting the length of the tether (longer or shorter), the tether tensioning force can be measure again, and then the tether can be re-pinned into the epicardial anchor device.

[1052] In some embodiments, there is provided a device for adjusting the length and/or tension of a tether for a tethered transcatheter prosthetic heart valve after a transcatheter valve implantation procedure in a patient. The device can include a positioning device for operatively engaging an epicardial anchor device, and the positioning device includes a positioning rod. The positioning rod member includes at a distal end of an elongate member a docking member that has a hinged frame that is connected to a circular platform having two bent locking tines or flanges located across from each other. The elongate member may or may not be hollow and includes a mechanism associated therewith for inserting or withdrawing a locking pin from a tether. The positioning device further includes a pin locking thumb wheel sub-component to actuate the pin locking mechanism that drives or removes a piercing pin on the epicardial anchor device into or from the tether. The positioning device further includes a transparent segment between the pin locking thumb wheel and a proximal end of the positioning device. The transparent segment has an implant position scale marked thereon. A proximal end of the positioning device also has a tether attachment pin vise. When the tether is threaded through the epicardial anchor device and the positioning device, and when the tether is drawn/pulled to the desired tension, e.g., such that the deployed valve seats firmly in the native annulus and any regurgitation seen on fluoroscopy or echocardiography is no longer present, the tether tensioning can be adjusted by visually observing the tether within the transparent segment of the positioning device and comparing the longitudinal distance travelled against an implant position scale. After the tether is suitably located, the pin locking thumb wheel is actuated and the pin locks the tether in place on the epicardial anchor device. The docking member is then disengaged from the epicardial anchor device.

[1053] In some embodiments, there is provided a tether release tool that has a distal tip that includes a shaped anchor device-engagement tip, a distal opening and a passageway in fluid communication with an angled tether capture/recapture access port. The angled tether capture/recapture access port allows a tether to be captured and released from a locked position, and the shaped anchor device-engagement tip is configured to fit within a similarly shaped portion of an epicardial anchor device.

[1054] In some embodiments, there is provided a method of tethering a prosthetic heart valve during a transcatheter valve replacement procedure that includes deploying a transcatheter prosthetic heart valve in a patient using as an anchor an adjustable tether that is anchored within the heart between an apically affixed epicardial anchor device and a stent-based fastening system (e.g., attached to the prosthetic heart valve). The transcatheter prosthetic heart valve includes an expandable tubular stent having a cuff and an expandable internal leaflet assembly. The cuff includes wire covered with stabilized tissue or synthetic material, and the leaflet assembly is disposed within the stent and includes stabilized tissue or synthetic material.

[1055] In some embodiments, an epicardial anchor device for anchoring a transluminal (transventricular) suture/tether includes a substantially rigid suturing disk having a tether-capture mechanism such as an axial tunnel, a winding channel, or a functional equivalent, and a tether locking mechanism such as a locking pin or screw that intersects the axial tunnel, a locking pin or screw operatively associated with the winding channel, a cam device like a rope lock that grips the tether by compression between two cams or a cam and fixed locking wall, a metal compression fastener, a tooth and pawl device, various combinations of the above, or a functional equivalent thereof.

[1056] In another embodiment, an epicardial anchor device for anchoring a transluminal suture includes a substantially rigid suturing disk having an axial tunnel, a locking pin locking pin tunnel that intersects the axial tunnel, a locking pin operatively associated with the locking pin tunnel, one or more radial channels that do not intersect with the axial tunnel and that do not intersect the locking pin tunnel, and a winding channel circumferentially disposed within a perimeter sidewall of the disk.

[1057] In some embodiments, an epicardial anchor device further includes a polyester velour coating. In some embodiments, the one or more radial channels includes four radial

channels. In some embodiments, the one or more radial channels each have an enlarged axial keyhole tunnel.

[1058] In some embodiments, an epicardial anchor device includes a flexible pad operatively associated with the rigid tethering/suturing disk, and the flexible pad has a through-hole longitudinally aligned with the axial tunnel. In some embodiments, the epicardial anchor device further includes a sleeve gasket operatively associated with the rigid tethering/suturing disk, and the sleeve gasket has a lumen longitudinally aligned with the axial tunnel. In some embodiments, the device further includes a sleeve gasket attached to the rigid tethering/suturing disk and a flexible pad attached to the sleeve gasket. In such an embodiment, the sleeve gasket has a lumen longitudinally aligned with the axial tunnel of the tethering/suturing disk, and the flexible pad has a through-hole longitudinally aligned with both the lumen of the sleeve gasket and the axial tunnel of the tethering/suturing disk.

[1059] In some embodiments, a device for anchoring a transluminal tethering/suture includes a substantially rigid tethering/suturing disk, a sleeve gasket connected to the tethering/suturing disk, and a flexible pad connected to the sleeve gasket. The substantially rigid tethering/suturing disk has an axial tunnel, a locking pin tunnel that intersects the axial tunnel, a locking pin operatively associated with the locking pin tunnel, one or more radial channels that do not intersect with the axial tunnel and that do not intersect the locking pin tunnel, and a winding channel circumferentially disposed within a perimeter sidewall of the disk. The sleeve gasket is in longitudinal alignment with the axial tunnel, and the flexible pad has a through-hole longitudinally aligned with both the lumen of the sleeve gasket and the axial tunnel of the tethering/suturing disk.

[1060] In another embodiment, an epicardial anchor device for anchoring a transluminal suture includes a substantially rigid tethering/suturing disk having an axial tunnel, a locking pin tunnel that intersects the axial tunnel, and a locking pin operatively associated with the locking pin tunnel.

[1061] In some embodiments, a method for anchoring a transluminal suture includes affixing a transluminal suture to an epicardial anchor device as described herein, and positioning the epicardial anchor device external to a body lumen. The transluminal tether/suture extends from within the lumen to the epicardial anchor device.

[1062] In another embodiment, a tether and epicardial anchor device as described herein further includes a tether tension load measuring device operatively associated with the tether. In some embodiments, a tension sensor includes one or more electronic strain gage transducers. The tension sensor can be configured for dynamic tension, static tension, or both dynamic and static tension measurement. In some embodiments, the tether is loaded with a specific tension, such as, for example, 1.0 to 4.0 lbs.

[1063] In another embodiment, there is provided a device and exemplary method for monitoring and/or controlling tether load during implant positioning using a fluid chamber device described in more detail below. A force sensor device having an annular fluid chamber is installed on the proximal end of a positioning device. This chamber is connected to a pressure transducer and then connected to a monitoring display. In some embodiments, a mechanical indicator can be used in conjunction therewith. A spring device may be connected to a mechanical tension meter to show load range. In some embodiments, the force sensor device remains as an integral part of the epicardial fastening pad assembly and is not removed after the tether tensioning is performed.

[1064] In some embodiments, a sterile surgical kit can be provided. The sterile surgical kit can contain a transcatheter delivery system, an epicardial anchor device and/or a transcatheter prosthetic valve.

[1065] In another embodiment, there is provided method of treating mitral or tricuspid regurgitation in a patient, which includes surgically deploying an adjustable-tethered prosthetic heart valve into the mitral or tricuspid annulus of the patient.

[1066] In another embodiment, the space between the cuff tissue and cuff Dacron liner (inside-outside) may be used to create a cuff that is expandable, swellable or may be inflated, and which provides an enhanced level of sealing of the cuff against the annular tissue.

[1067] Various embodiments described herein address problems concerning valve delivery and deployment, valve compliance, perivalvular leaking, hemodynamic issues such as LVOT interference, clotting, cardiac remodeling and so forth.

[1068] In some embodiments described herein, a tethering system for a prosthetic mitral valve is provided that is designed to maintain integrity to about 800 million cycles, or about 20 years. The use of a compressible prosthetic valve delivered via transcatheter endoscope

techniques addresses various delivery issues. Deployment is addressed through the use of a prosthetic valve having a shape that features a tubular stent body that contains leaflets and an atrial cuff. This allows the valve to seat within the mitral annulus and be held by the native mitral leaflets. The use of a flexible valve attached using an apical tether provides compliance with the motion and geometry of the heart. The geometry and motion of the heart are well-known as exhibiting a complicated biphasic left ventricular deformation with muscle thickening and a sequential twisting motion. The additional use of the apically secured ventricular tether helps maintain the prosthetic valve's annular position without allowing the valve to migrate, while providing enough tension between the cuff valve annulus to reduce and eliminate perivalvular leakage. The use of an adjustable tether or an adjustable paired-tether that is attached to an apical location can reduce or eliminate the cardiac muscle remodeling that has been witnessed in prior art devices. Some prior art devices can have a problem with unwanted change in tissue at the anchoring locations, as well as heart-generated migration of the original anchoring locations to new locations that reduce or destroy the prior art valve's effectiveness. The use of a compliant valve prosthesis and the special shape and features help reduce or eliminate clotting and hemodynamic issues, including LVOT interference problems. Many prior art valves were not designed with an awareness of, or were not able to address, problems with blood flow and aorta/aortic valve compression issues.

[1069] Structurally, a prosthetic heart valve as used with the apparatus and methods described herein can include a self-expanding tubular body having a cuff at one end and one or more tethers attached at the other end. Disposed within the tubular body is a leaflet assembly that contains the valve leaflets, and the valve leaflets can be formed from stabilized tissue or other suitable biological or synthetic material. In one embodiment, the leaflet assembly may include a wire form where a formed wire structure is used in conjunction with stabilized tissue to create a leaflet support structure which can have anywhere from 1, 2, 3 or 4 leaflets, or valve cusps disposed therein. In another embodiment, the leaflet assembly is wireless and uses only the stabilized tissue and stent body to provide the leaflet support structure, without using wire, and which can also have anywhere from 1, 2, 3 or 4 leaflets, or valve cusps disposed therein.

[1070] The upper cuff portion may be formed by heat-forming a portion of a tubular Nitinol[®] braided (or similar) stent such that the lower portion retains the tubular shape, but

the upper portion is opened out of the tubular shape and expanded to create a widened collar structure that may be shaped in a variety of functional regular or irregular funnel-like or collar-like shapes. In one embodiment, the entire structure is formed from a laser-cut stent and collar design, as described further herein.

[1071] As used in this specification, the singular forms “a,” “an” and “the” include plural referents unless the context clearly dictates otherwise. Thus, for example, the term “a member” is intended to mean a single member or a combination of members, “a material” is intended to mean one or more materials, or a combination thereof.

[1072] As used herein, the words “proximal” and “distal” refer to a direction closer to and away from, respectively, an operator of, for example, a medical device. Thus, for example, the end of the medical device closest to the patient’s body (e.g., contacting the patient’s body or disposed within the patient’s body) would be the distal end of the medical device, while the end opposite the distal end and closest to, for example, the user (or hand of the user) of the medical device, would be the proximal end of the medical device.

[1073] A prosthetic mitral valve can be anchored to the heart at a location external to the heart via one or more tethers coupled to an anchor device, as described herein. For example, the tether(s) can be coupled to the prosthetic mitral valve and extend out of the heart and be secured at an exterior location (e.g., the epicardial surface) with an anchor device, as described herein. An anchor device as described herein can be used with one or more such tethers in other surgical situations where such a tether may be desired to extend from an intraluminal cavity to an external anchoring site. Various different types and/or configurations of an anchor device (also referred to herein as “epicardial anchor device” or “epicardial pad” or “pad”) can be used to anchor a prosthetic mitral valve in the methods described herein. For example, any of the epicardial anchor devices described in PCT International Application No. PCT/US2014/049218, filed July 31, 2014, entitled “Epicardial Anchor Devices and Methods,” (referred to herein as “the ‘218 PCT application”), can be used.

[1074] FIG. 1 is a schematic cross-sectional illustration of the left ventricle LV and left atrium LA of a heart H having a transcatheter prosthetic mitral valve PMV deployed therein and an epicardial anchor device EAD as described herein securing the prosthetic mitral valve PMV in place. FIG. 1 illustrates the prosthetic mitral valve PMV seated into the native valve

annulus and held there using an atrial cuff AC of the prosthetic mitral valve PMV and a ventricular tether T secured with attachment portions Tp to the prosthetic mitral valve PMV and to the epicardial anchor EAD. The epicardial anchor device EAD can be various different shapes, sizes, types and configurations, for example, the EAD can be an epicardial anchor device such as those described in the '218 PCT application.

Further, the prosthetic mitral valve PMV and the tether T can be, for example, a prosthetic mitral valve and tether, respectively, as described in the '218 PCT application or other suitable types and configurations.

[1075] FIG. 2 is a schematic illustration of an epicardial anchor device 100 (also referred to herein as “anchor device” or “epicardial anchor”) according to an embodiment. The anchor device 100 can be used to anchor or secure a prosthetic mitral valve PMV deployed between the left atrium LA and left ventricle LV of a heart H. The anchor device 100 can be used, for example, to anchor or secure the prosthetic mitral valve PMV via a suturing tether 128 as described above with respect to FIG. 1. The anchor device 100 can also seal a puncture formed in the ventricular wall (not shown in FIG. 2) of the heart during implantation of the prosthetic mitral valve PMV. The anchor device 100 can also be used in other applications to anchor a medical device (such as any prosthetic atrioventricular valve or other heart valve) and/or to seal an opening such as a puncture.

[1076] The anchor device 100 can include a pad (or pad assembly) 120, a tether attachment member 124 and a locking pin or locking pin assembly 126. The pad 120 can contact the epicardial surface of the heart and can be constructed of any suitable biocompatible surgical material. The pad 120 can be used to assist the sealing of a surgical puncture formed when implanting a prosthetic mitral valve.

[1077] In some embodiments, the pad 120 can be made with a double velour material to promote ingrowth of the pad 120 into the puncture site area. For example, pad or felt pledgets can be made of a felted polyester and may be cut to any suitable size or shape, such as those available from Bard[®] as PTFE Felt Pledgets having a nominal thickness of 2.87mm. In some embodiments, the pad 120 can be larger in diameter than the tether attachment member 124. The pad 120 can have a circular or disk shape, or other suitable shapes.

[1078] The tether attachment member 124 can provide the anchoring and mounting platform to which one or more tethers 128 can be coupled (e.g., tied or pinned). The tether

attachment member 124 can include a base member (not shown) that defines at least a portion of a tether passageway (not shown) through which the tether 128 can be received and pass through the tether attachment member 124, and a locking pin channel (not shown) through which the locking pin 126 can be received. The locking pin channel can be in fluid communication with the tether passageway such that when the locking pin 126 is disposed in the locking pin channel, the locking pin 126 can contact or pierce the tether 128 as it passes through the tether passageway as described in more detail below with reference to specific embodiments.

[1079] The locking pin assembly 126 can be used to hold the tether 128 in place after the anchor device 100 has been tightened against the ventricular wall and the tether 128 has been pulled to a desired tension. For example, the tether 128 can extend through a hole in the pad 120, and through the tether passageway of the tether attachment member 124. The locking pin 126 can be inserted or moved within the locking pin channel 134 such that it pierces or otherwise engages the tether 128 as the tether 128 extends through the tether passageway of the tether attachment member 124. Thus, the locking pin 126 can intersect the tether 128 and secure the tether 128 to the tether attachment member 124.

[1080] The tether attachment member 124 can be formed with, a variety of suitable biocompatible material. For example, in some embodiments, the tether attachment member 124 can be made of polyethylene, or other hard or semi-hard polymer, and can be covered with a polyester velour to promote ingrowth. In other embodiments, the tether attachment member 124 can be made of metal, such as, for example, Nitinol[®], or ceramic materials. The tether attachment member 124 can be various sizes and/or shapes. For example, the tether attachment member 124 can be substantially disk shaped.

[1081] In use, after a PMV has been placed within a heart, the tether extending from the PMV can be inserted into the tether passageway of the anchor device 100 and the tension on the tether attachment device can be adjusted to a desired tension. Alternatively, in some cases, the tether extending from the PMV can be coupled to the anchor device 100 prior to the PMV being placed within the heart. The anchor device 100 (e.g., some portion of the anchor device such as the tether attachment member 124, or the lever arm or hub depending on the particular embodiment) can be actuated such that the locking pin 126 intersects the tether passageway and engages a portion of the tether disposed within the tether passageway, securing the tether to the tether attachment member. In some embodiments, prior to inserting

the tether into the tether passageway, the anchor device 100 can be actuated to configure the anchor device 100 to receive the tether. For example, if the tether attachment member includes a lever arm movably coupled to the base member, the lever arm may need to be moved to an open position to allow the tether to be inserted. In some embodiments, the anchor device 100 can be actuated by rotating a hub relative to a base member of the tether attachment member 124 such that the locking pin 126 is moved from a first position in which the locking pin is spaced from the tether passageway and a second position in which the locking pin intersects the tether passageway and engages or pierces the portion of the tether.

[1082] FIG. 3 is a schematic illustration of an embodiment of a positioning device 142 that can be used to position the epicardial anchor device 100 and measure the tension applied to a tether 128 attached to a prosthetic mitral valve (not shown in FIG. 3) to be anchored by the epicardial anchor device 100. The positioning device 142 includes a handle assembly 144, an elongate member 145, a docking member 146, and a tether securing member 147. In some embodiments, the positioning device 142 can include a force sensor device 148, which can communicate with a transducer 149, which in turn can communicate with an electronic device 141 to display the output of the force sensor device 148. In some embodiments, the transducer 149 can be incorporated within the force sensor device 148. In some embodiments, the force sensor device 148 can be coupled to a data acquisition module rather than a transducer. The electronic device 141 can be, for example, a monitor or display of a computer, such as a laptop computer or a desktop computer, or a handheld electronic device such as a tablet, phone or other electronic device configured to receive and display the output of the force sensor device 148.

[1083] The positioning device 142 can include other various components that can be for example coupled to or incorporated within the handle assembly 144 or another component of the positioning device 142. The docking member 146 can be used to releasably couple the epicardial pad 100 to the positioning device 142 and can be actuated by one or more components of the positioning device 142. The tether securing device 147 can include, for example, a vice mechanism used to lock the tether 128 at a desired position. In some embodiments, the tether securing device 147 can include a pinning device that can pierce the tether 128 to secure the tether 128 in the desired position. More detailed descriptions of various components of embodiments of a positioning device 142 are described below.

[1084] FIGS. 4-12 illustrate an epicardial anchor device according to an embodiment. An epicardial anchor device 200 includes a tether attachment member 224, a pad assembly 220, a tube member 255 and a tube cover member 256. The tether attachment member 224 includes a base member 240, a hub 250, a retaining ring 252, a locking pin assembly 226, and a pin member 253. The locking pin assembly 226 includes a driver portion 246 and a piercing portion 249. The base member 240 defines a circumferential pad channel 242, a retaining channel 251 and a locking pin channel 234. The pad channel 242 can be used to couple the pad assembly 220 to the tether attachment member 224. The retaining channel 251 can receive an outer edge of the retaining ring 252, which is used to retain the hub 250 to the base member 240. The base member 240 also defines cutouts or detents 243, as shown for example, in FIGS. 5, 7 and 12.

[1085] The tube member 255 is coupled to the base member 240 and the base member 240, the hub 250 and the tube member 255 collectively define a tether passageway 235 through which a tether (not shown) can be received. The cover member 256 can be formed with a fabric material, such as for example, Dacron[®]. The tether channel 235 intersects the locking pin channel 234 and is in fluid communication therewith.

[1086] The pad assembly 220 includes a top pad portion 258, a bottom pad portion 259 and a filler member 257 disposed therebetween. The top pad portion 258 and the bottom pad portion 259 can each be formed with, for example, a flexible fabric material. The top pad portion 258 and the bottom pad portion 259 can each define a central opening through which the tube member 255 can pass through. A portion of the top pad portion 258 is received within the channel 242 of the base member 240 as shown, for example, in FIGS. 7-9.

[1087] An outer perimeter portion of the hub 250 is received within the retaining channel 251 such that the hub 250 can rotate relative to the base member 240 to actuate the locking pin assembly 226 as described in more detail below. As shown, for example, in FIGS. 10 and 11, the hub 250 includes arms 261 with protrusions 262. The protrusions 262 can be received within cutouts 243 of the base member 240 and act as a stop or limit to the rotation of the hub 250. The hub 250 defines slots 263 that enable the arms 261 to flex and allow the protrusions 262 to be moved in and out of the cutouts 243. As shown, for example, in FIGS. 9 and 10 the hub 950 defines a curved channel 250 on a bottom portion of the hub 950. The curved channel 250 is asymmetrical (or spiral) and receives the driver portion 246 of the locking pin assembly 226. As the hub 250 is rotated relative to the base member 240, the hub 250 acts as

a cam to move the locking pin assembly 226 linearly within the locking pin channel 234. The locking pin assembly 226 can be moved from a first position in which the piercing portion 249 is disposed outside of the tether passageway 235 as shown in FIGS. 7 and 8, and a second position in which the piercing portion 249 extends through the tether passageway 235 as shown in FIG. 9. The pin member 253 (see, e.g., FIG. 8) can be formed with a metal material that is more radio-opaque than the other components of the anchor device and thus visible to the user (e.g. physician) using conventional imaging modalities to enable the user to confirm that the locking pin assembly 226 has been fully moved to the second position.

[1088] In use, when the locking pin assembly 226 is in the first position, a tether (not shown) coupled to, for example, a prosthetic mitral valve and extending through a puncture site in the ventricular wall of a heart can be inserted through the tether passageway 235. The hub 250 can then be rotated 180 degrees to move the locking pin assembly 226 linearly within the locking pin channel 234 such that the piercing portion 249 extends through the tether passageway 235 and engages or pierces the tether, securing the tether to the tether attachment member 224. For example, the hub 250 also defines a driver receiving opening 210 configured to receive a mating portion of a positioning device (described below, e.g., with reference to positioning devices 242, 342 and 442). The positioning device can be used to rotate the hub and actuate the locking pin assembly 226. When the locking pin is in the first position, the protrusions 262 of the hub 250 are each disposed within one of the cutouts 243 of the base member 240 (i.e., a first protrusion is in a first cutout, and a second protrusion is in a second cutout). The hub 250 can then be rotated 180 degrees such that the protrusions 262 are moved out of the cutouts 243 of the base member 240 and at the end of the 180 degrees the protrusions 262 are moved into the other of the cutouts 243 of the base member 240 (i.e., the first protrusion is now in the second cutout, the second protrusion is now in the first cutout).

[1089] The base member 240 can also include cutout sections 266 and define side openings 267 (see, e.g., FIGS. 4 and 5) that can be used to couple a positioning device to the epicardial anchor device 200. For example, FIGS. 13 – 17B illustrate a positioning device 242 that can be used to deploy and position an epicardial anchor device such as anchor device 200.

[1090] As shown in FIG. 13, in this embodiment, the positioning device 242 includes an elongate member 245, a docking member 246 coupled to a distal end of the elongate member

245, a handle assembly 244 and a tether securing member 247. The handle assembly 244 includes a housing 254, a transparent tube segment 223 with indications disposed thereon, a tension member 229, a thumb dial 227, a release button 233 and a safety lever 231.

[1091] The handle assembly 245 is coupled to the tether securing device 247 with a rod member 264 (see, e.g., FIG. 15). The handle assembly 245 is also coupled to the elongate member 245, which is coupled to the docking member 246. The docking member 246 includes coupling arms 236 with coupling pins 238 extending inwardly from the coupling arms 236. The coupling pins 238 are configured to be received within the side openings 267 of the anchor device 200 described above, and the coupling arms 236 can engage the cutout sections 266 of the anchor device 200. The coupling arms 236 have hinged joints which are coupled to a disc member 239. The disc member 239 can be coupled to or incorporated with or monolithically formed with the elongate member 245. A spring 216 disposed between the disc member 239 and the arms 236 biases the coupling arms 236 in a closed position as shown, for example, in FIG. 13, 15 and 16. The coupling arms 236 can be moved to an open position (not shown) to allow for the anchor device 200 to be received between the coupling arms 236 to couple and release the anchor device 200 to and from the positioning device 242. Actuation of the docking member 236 is described in more detail below. An inner driver member 217 is movably disposed within a lumen defined by the elongate member 245 and extends through the docking member 246. The inner driver member 217 includes a shaped distal tip 237 that is configured to be matingly received within the driver receiving opening 210 of the anchor device 200. The inner driver member 217 is operatively coupled to the thumb dial 227 of the positioning device 242 and can be used to actuate the locking pin assembly 226 of the anchor device 200 to secure a tether to the anchor device 200, as described below.

[1092] The safety lever 231 is hingedly coupled to the housing 254 and can be moved from a first position as shown, for example, in FIG. 13, in which the safety lever 231 prevents the release button 233 from moving and a second position (not shown) in which the safety lever 231 is pivoted or moved in a direction upward away from the elongate member 245 such that the release button 223 can be moved as desired as described in more detail below.

[1093] In use, a tether (not shown) extending from a prosthetic mitral valve and outside of the heart can be inserted through the epicardial anchor device 200 and threaded through a

lumen of the inner driver member 217, through the handle assembly 244, and out through the tether securing device 247.

[1094] To releasably couple and uncouple the anchor device 200 to and from the positioning device 242, the safety lever 231 is moved to its second position in which the release button 233 is free to move. The release button 233 is fixedly coupled to the elongate member 245 such that as the release button is moved distally, the elongate member 245 moves distally, and in turn the disc member 239 moves distally compressing the spring 216 and actuating the hinged coupling arms 236 of the docking member 246 to open wide enough such that the anchor device 200 can be placed therebetween. The distal tip 237 of the driver member 217 is received within the opening 210 of the anchor device 200. The release button 233 can then be moved proximally to allow the coupling arms 236 to move back to their biased closed position (e.g., closer together) and be inserted into the side openings 267 of the anchor device 200. The safety lever 231 can then be moved back to its first position, as shown in FIG. 13.

[1095] With the anchor device 200 coupled to the positioning device 242, the anchor device 200 can be positioned at a desired location on the outer surface of the ventricular wall of the heart, such as for example, at the apex. The tether extending through the positioning device 242 and out the proximal end of the positioning device 242 can be pulled proximally to a desired tension. When the tether is drawn/pulled to the desired tension, e.g., such that the deployed prosthetic valve seats firmly in the native annulus and any regurgitation seen on fluoroscopy or echocardiography is no longer present, the practitioner can fine tune the tensioning by visually observing the tether within the transparent tube segment 223 and compare the longitudinal distance travelled against an implant position scale. When the tether is suitably located, the locking pin assembly 226 of the anchor device 200 can be actuated by the positioning device 242 to lock the tether in place on the epicardial anchor device 200. For example, the thumb dial 227, which is operatively coupled to the driver member 217, can be rotated to actuate the locking pin assembly 226 of the anchor device 200 to pierce the tether and secure the tether to the anchor device 200.

[1096] Prior to pinning the tether to the anchor device 200, it may be desirable to make small adjustments or fine tuning to the position of the anchor device 200 and/or to the tension of the tether. To make such adjustments or fine tuning, the tether securing device 247 can be used to secure the tether at a fixed position on the positioning device 242, such that the

anchor device 200 can be pushed distally snug to the outer wall of the heart. For example, in this embodiment, the tether securing device 247 includes a collet 212 (see, e.g., FIGS. 15 and 17A) that provides a friction fit against the tether when the tether securing device 247 is rotated. If an adjustment to the tension of the tether and/or to the position of the anchor device 200 is desired, with the tether securing device 247 holding the tether in a fixed position, the tension member 229 can be actuated to allow the handle assembly 244, elongate member 245 and docking member 246 to be moved distally relative to the rod member 264 to which the tether securing device 247 is coupled. For example, as shown in FIGS. 17A and 17B, grooved teeth 265 of the rod member 264 allow the handle assembly 244 to be incrementally moved distally. Alternatively, the push buttons 219 on the tension member 229 can be depressed which will release the grooved teeth 265 and allow the handle assembly 244 to be slid freely relative to the rod member 264.

[1097] When the anchor device and tether have been secured in a desired position and at a desired tension, the positioning device 242 can be actuated to pin the tether to the anchor device 200 as described above, and then the epicardial anchor device 200 can be released from the positioning device 242. The portion of the tether extending from the anchor device 200 can be cut to a desired length and/or tied off.

[1098] FIGS. 18-21 illustrate another embodiment of a positioning device that can be used to position an epicardial anchor device such as anchor device 200. As with the previous embodiment, the positioning device 342 includes an elongate member 345, a docking member 346 coupled to a distal end of the elongate member 345, and a handle assembly 344 coupled to the elongate member 345. The handle assembly 344 includes a housing 354, a transparent tube member 323 with indications disposed thereon, a tension member 329, a thumb dial 327, a release button 333 and a safety lever 331. Each of these components can be the same as or similar to the corresponding components of positioning device 242 and are therefore not discussed in detail with respect to this embodiment.

[1099] In this embodiment, the positioning device 342 also includes a force sensor device 348 coupled at a proximal end of the positioning device 342. The force sensor device 348 can be coupled to the housing 344 via a rod member 364 similar to the rod member 264. The force sensor device 348 includes a sensor housing 369 defining an interior region that receives a load cell 368. In some embodiments, the load cell can include, for example a piezoelectric sensor. In some embodiments the load cell 368 can include miniature strain

gauges. The load cell 368 can be electrically coupled to a transducer (not shown) or a data acquisition module (not shown) via a cable 311, which in turn can communicate with an electronic device (not shown) configured to display the output of the force sensor device 348 as described above with respect to FIG. 3. The electronic device can be, for example, a monitor or display of a computer, such as a laptop computer or a desktop computer, or a handheld electronic device such as a tablet, phone or other electronic device configured to receive and display the results of the force sensor device 348.

[1100] The positioning device 342 can also include a tether securing device 347 coupled proximally to force sensor device 348. The tether securing device 347 includes a collet (not shown) that provides a friction fit against a tether when the tether securing device 347 is rotated as described for the previous embodiment. As shown in the schematic illustration of FIG. 21, the rod member 364 can extend through the force sensor device 348 and the tether securing device 347 can be coupled thereto.

[1101] In use, as with the previous embodiment, a tether (not shown) extending from a prosthetic mitral valve and outside of the heart can be inserted through an epicardial anchor device, threaded through the elongate member 345, through the handle assembly 344, and out through the tether securing device 347. The anchor device can be releasably coupled to the positioning device 342 in the same manner as described above for positioning device 242 and the locking pin assembly of the anchor device can be actuated to pin the tether to the anchor device as described above.

[1102] The anchor device 200 can be positioned at a desired location on the outer surface of the ventricular wall of the heart, such as for example, at the apex. The tether extending through the positioning device 342 can be pulled proximally to a desired tension. In this embodiment, the tension on the tether can be measured and displayed for the practitioner. For example, tether securing device 347 exerts a compressive force on the load cell 368 as the tether is being pulled through. The compressive force displaces the load cell, which causes a deflection of the load cell which is detected by the sensor(s) within the load cell 368. The deflection data is sent to the data acquisition module which in turn provides pressure data to be viewed on an electronic display. When the desired tension on the tether is achieved, the tether securing device 347 can be used to secure the tether at a fixed position relative to the positioning device 342 as described above.

[1103] If an adjustment to the tension of the tether and/or to the position of the anchor device on the tether is desired, with the tether securing device 347 holding the tether in a fixed position, and while holding the tether securing device 347, the tension member 329 can be actuated to allow the handle assembly 344, elongate member 345 and docking member 346 to be moved distally relative to the rod member 364 and tether securing device 347. For example, as previously described, the tension member 329 can be used to incrementally move the handle assembly 344 distally or push buttons 319 on the tension member 329 can be depressed which will release grooved teeth 365 on the rod member 364 and allow the handle assembly 344 to be slid freely relative to the rod member 364.

[1104] When the anchor device and tether have been secured in a desired position and at a desired tension, the positioning device 442 can be actuated to release the epicardial anchor device. The portion of the tether extending from the anchor device can be cut to a desired length and/or tied off.

[1105] FIGS. 22-28 illustrate a positioning device 442 according to another embodiment. The positioning device 442 can be configured the same as or similar to and provide the same or similar functions as the above described embodiments. The positioning device 442 includes a docking member 446 coupled to a distal end of an elongate member 445, a handle assembly 444 and a force sensor device 448. The positioning device 442 can also include a tether securing device (not shown) that can be the same as or similar to the tether securing devices described above. The handle assembly 444 includes a housing 454 having a transparent segment 423 with indications disposed thereon, a tension member 429, a switch 427, a release knob 433 and a safety lever 431.

[1106] The handle assembly 445 is coupled to the elongate member 445, which is coupled to the docking member 446. The docking member 446 includes coupling arms 436 with coupling pins 438 extending inwardly from the coupling arms 436. As with the previous embodiments, the coupling pins 438 are configured to be received within the side openings of an anchor device such as anchor device 200 described above. The coupling arms 436 can also engage the cutout sections of the anchor device as described above. The coupling arms 436 have hinged joints which are coupled to a disc member 439 which is coupled to or incorporated or monolithically formed with the elongate member 445. A spring 416 is disposed between the disc member 439 and the arms 436 and biases the arms 436 in a closed position as shown, for example, in FIG. 13, 15 and 16. The coupling arms 436 can be moved

to an open position (not shown) to allow for the anchor device to be received between the coupling arms 436 to couple and release the anchor device to and from the positioning device 442. Actuation of the docking member 436 is described in more detail below. An inner driver member 417 is movably disposed within a lumen defined by the elongate member 445 and extends through the docking member 446. The inner driver member 417 includes a shaped distal tip 437 that is configured to be matingly received within a driver receiving opening of the anchor device as described above. The inner driver member 417 is operatively coupled to the switch 427 of the positioning device 442 and can be used to actuate the locking pin assembly of the anchor device to secure a tether to the anchor device, as described above for previous embodiments.

[1107] The safety lever 431 can be moved from a first position as shown in FIGS. 22, 24 and 25 in which the safety lever 431 prevents the release button 433 from moving and a second position (not shown) in which the safety lever 433 is moved in a direction downward away from the elongate member 445 such that the release button 433 can be moved as desired as described in more detail below.

[1108] As shown in FIGS. 26-30, in this embodiment, the force sensor device 448 includes a sensor housing 470, a fluid chamber 472 and a load washer 474. The fluid chamber 472 defines an interior region that can contain a fluid and that is in fluid communication with a conduit 476. The fluid chamber 472 is received within the sensor housing 470 and the conduit 476 extends out of the sensor housing 470 through an opening 475 defined by the sensor housing 470. The load washer 474 is disposed over the fluid chamber 472 and is coupled to the sensor housing 470 with pins 471 such that the load washer 474 can move within slots 477 defined by the sensor housing 470. This allows for the fluid chamber 472 to reduce and expand in size within the interior region defined collectively by the sensor housing 470 and the load washer 474. A fluid port connector 473 is coupled to the conduit 476. The fluid port connector 473 can be for example, a Luer connector. The fluid port connector 473 can be coupled to a pressure transducer (not shown) which in turn can be coupled to a device that can be used to display pressure readings received from the pressure transducer. In some embodiments, the pressure transducer can be incorporated within the force sensor device 448, or coupled directly to or proximate to the force sensor device 448. During use, force is exerted on the load washer 474 which in turn exerts a compressive force on the fluid chamber 472 causing the pressure of the fluid in the interior

region of the fluid chamber 472 to be increased. This increased pressure can be communicated through the fluid from the fluid chamber 472 to and through the conduit 476. The force sensor device 448 can be used to measure the load on a tether extending through the positioning device 442. For example, the positioning device 442 can include a tether securing member (not shown) that can be configured the same as or similar to the tether securing device 247 described above. In a similar manner as shown for force sensor device 448 (see, e.g., FIG. 21), the rod member 464 can extend through the force sensor device 448 and the tether securing device can be coupled to the rod member 465 and disposed on a proximal side of the force sensor device 448 in contact with the load washer 474. As the tether is pulled through to a desired tension, the tether securing device exerts a force on the load washer 474.

[1109] In use, a tether (not shown) extending from a prosthetic mitral valve and outside of the heart can be inserted through an epicardial anchor device 400 (see, FIG. 22) and threaded through a lumen of the inner driver member 417, through the handle assembly 444, and out through the tether securing device (not shown). For purposes of the following description, the epicardial anchor device 400 can be the same as the epicardial anchor device 200 described above.

[1110] To releasably couple and uncouple the anchor device 400 to and from the positioning device 442, the safety lever 431 is moved to its second position in which the release button 433 is free to move. The release button 433 is fixedly coupled to the elongate member 445 such that as the release button 433 is moved distally, the elongate member 445 moves distally, and in turn the disc member 439 moves distally compressing the spring 416 and actuating the hinged coupling arms 436 of the docking member 446 to open wide enough such that the anchor device 400 can be placed therebetween. The distal tip 437 of the driver member 417 is received within the mating opening of the anchor device 400 as described above for anchor device 200. The release knob 433 can then be moved proximally to allow the coupling arms 436 to move back to their biased closed position (e.g., closer together) and be inserted into the side openings of the anchor device 400. The safety lever 431 can then be moved back to its first position, as shown in FIGS. 24 and 25.

[1111] With the anchor device 400 coupled to the positioning device 442, the anchor device 400 can be positioned at a desired location on the outer surface of the ventricular wall of the heart, such as for example, at the apex. The tether extending through the positioning

device 442 and out the proximal end of the positioning device 442 can be pulled proximally to a desired tension. When the tether is drawn/pulled to the desired tension, e.g., such that the deployed prosthetic valve seats firmly in the native annulus and any regurgitation seen on fluoroscopy or echocardiography is no longer present, the practitioner can fine tune the tensioning by visually observing the tether within the transparent segment 423 and comparing the longitudinal distance travelled against an implant position scale. Further, as shown in FIG. 29, the transparent segment 423 includes markings or indications 415. In this example, the markings 415 include indications between 5 and 15 centimeters. Different indications and/or increments can be used as appropriate. A distal portion of the rod member 464 can be viewed through the transparent segment 423 and includes an indicator 418 at a distal end of the rod member 464. The indicator 418 can be a marking on the rod member 464 or a separate component coupled to the rod member 464. In some embodiments, the indicator 418 can be color coded. The indicator 418 shows the location of the rod member 464 as the rod member 464 is moved in a proximal and distal direction and corresponds to a distance between the bottom surface of the epicardial pad device 400 that contacts the heart and the annulus of the heart valve. For example, the markings 415 can be used to identify the location of the indicator 418 on the distal end of the rod member 464. The distance between the bottom surface of the epicardial pad device 400 that contacts the heart and annulus of the heart can be determined based on a known length of the tether. For example, a proximal end portion of the tether extending out of the positioning device 442 can have a marker 414 (see FIG. 39 illustrating a tether 428 with a marker 414 coupled thereto). The marker 414 can be for example, a stainless steel hypotube or band crimped or swaged onto the tether. The marker 414 on the tether can indicate a preset distance from where the prosthetic mitral valve is seated in the annulus. For example, the marker 414 can be a set distance of 40 mm from where the tether is attached at the cuff of the prosthetic mitral valve. From this, when the tether is extended through the positioning device 442, depending on the tension applied to the tether, the location of the indicator 418 on the rod member 464 can represent the distance between the epicardial pad device 400 that contacts the heart and annulus of the heart.

[1112] When the tether is suitably located, the locking pin assembly of the anchor device 400 can be actuated by the positioning device 442 to lock the tether in place on the epicardial anchor device 400. For example, the switch 427, which is operatively coupled to the driver member 417, can be actuated to rotate the driver member 417 and actuate the locking pin assembly of the anchor device 400 to pierce the tether and secure the tether to the anchor

device 400. In some embodiments, the switch 427 can be moved or flipped 180 degrees. For example, the driver member 417 can be moved 180 degrees to rotate the driver inward to actuate the pin locking assembly of the anchor device 400 and secure the tether, and then back 180 degrees to move the driver member 417 in the opposite direction to release the tether.

[1113] Prior to pinning the tether to the anchor device 400, it may be desirable to make small adjustments or fine tuning to the position of the anchor device 400 and/or to the tension of the tether. To make such adjustments or fine tuning, the tether securing device (not shown) can be used to secure the tether at a fixed position on the positioning device 442, such that the anchor device 400 can be pushed distally snug to the outer wall of the heart in a similar manner as described above with respect to positioning device 242. For example, in this embodiment, the rod member 464 can move proximally and distally relative to the handle assembly 444. While holding the tether securing device, the tension member 429 can be actuated (e.g., rotated) such that the rod member 464 rotates proximally with the tether securing device (not shown). For example, the tension member 429 can be coupled to the rod member 464 such that rotating of the tension member 429 causes the rod member to move proximally or distally depending on the direction of rotation of the tension member 429. This can provide the ability to make fine adjustments to the tension on the tether. In addition, the release button(s) 419 on the tension member 429 can be pressed to allow the tension member 429 to disengage from the teeth 465 of the rod member 464 and be freely slid relative to the rod member 464. In this manner, the tension member 429 can be slid distally, which in turn moves the handle assembly 444, elongate member 445 and docking member 446 distally relative to the rod member 464 and tether securing device.

[1114] As with the previous embodiment, the tension on the tether can be measured and displayed for the practitioner via the force sensor device 448. For example, as described above, the tether securing device (not shown) can exert a compressive force on the load washer 474 as the tether is being pulled through.

[1115] When the anchor device and tether have been secured in a desired position and at a desired tension, the positioning device 442 can be actuated to pin the tether to the anchor device 400 as described above, and then the epicardial anchor device 400 can be released from the positioning device 442. The portion of the tether extending from the anchor device 400 can be cut to a desired length and/or tied off.

[1116] FIG. 31 illustrates a tension limiting device (also referred to as “tensioner”) that can be included in the positioning devices described herein. The tensioner 480 can be incorporated within, for example, the tension member 429’ and can be used to limit the amount of load (e.g. tension T) that can be set during prosthetic valve implantation. The tensioner 477 includes ratchet members 478 and 479 that skip over each other when maximum tension on the lead screw is achieved. A spring 483 is coupled to the rod member 464 and applies tension on the ratchet members 478 and 479. The ratchet member 479 can be coupled to the housing of the tension member 429 and can move axially along the rod member 464. The ratchet member 478 includes inner teeth that engage the teeth 465 of the rod member 464 such that the ratchet member 478 can be moved along the rod member 464 as the tension member 429 is rotated. For example, as the tension member 429 is rotated to adjust the tension on the tether, the ratchet member 479 will move with the tension member 429 and the ratchet member 478 will slide relative to the ratchet member 479 until the tension on the tether exceeds a set value, at which point the tensioner 480 will act like a slip clutch, preventing further tensioning. The tension limit can be a preset value of the device or can be set according to the particular procedure and/or patient.

[1117] FIGS. 36 and 37 illustrate an alternative embodiment of a force sensor device 648 that can be included on a positioning device described herein. The force sensor device 648 is similar to the force sensor device 448 and can function in the same or similar manner as the force sensor device 448. The force sensor device 648 includes a sensor housing 670, a fluid chamber 672 and a load washer 674. The fluid chamber 672 defines an interior region that can contain a fluid and that is in fluid communication with a conduit 676. The fluid chamber 672 is received within the sensor housing 670 and the conduit 676 extends out of the sensor housing 670 through an opening 675 defined by the sensor housing 670. The load washer 674 is disposed over the fluid chamber 672 and is coupled to the sensor housing 670 with a retainer 686 such that the load washer 674 can move or float relative to the sensor housing 670. For example, the load washer includes a perimeter flange (not shown) on which the retainer 686 rests on top of the sensor housing 670. This allows for the fluid chamber 672 to reduce and expand in size within the interior region defined collectively by the sensor housing 670 and the load washer 674. A spring 688 and adjuster screw 684 are disposed within an opening 690 (FIG. 38) defined in the sensor housing 670 and can be used to tune the pressure reading at a fixed load. The opening 690 is also used to couple the force sensor device 648 to a rod member (e.g., 464) of a positioning device (e.g., 642).

[1118] In this embodiment, a tether (not shown) extending through the positioning device to which the force sensor device 648 is coupled, extends through the rod member of the positioning device, through the adjuster screw 684 and spring 688, through load washer 674 and out a proximal opening 691 defined in the load washer 674 at a proximal end of the force sensor device 648. In this embodiment, a pinning mechanism incorporated into the force sensor device 648 can be used to pierce the tether and secure the tether to the force sensor device 648. The pinning mechanism includes a pin holder 685 coupled to a pin 687. The pin holder 685 can be manually moved inward to actuate or move the pin 687 inwardly into the opening 691 (see., e.g., FIG. 38) to pierce a tether extending therethrough.

[1119] A fluid port connector 673 is coupled to the conduit 676. The fluid port connector 673 can be for example, a Luer connector. The fluid port connector 673 can be coupled to a pressure transducer 649 via a conduit (not shown) which is disposed within a holder portion 689 defined in the sensor housing 670. The pressure transducer 649 being incorporated within the force sensor device 648 can compensate for tool height changes during a procedure that could change the pressure reading. The pressure transducer 649 can in turn be coupled to a device that can be used to display pressure readings received from the pressure transducer 649.

[1120] In this embodiment, during use, when the tether is pierced by the pin 687, the load is transferred to the load washer 674, which in turn exerts a compressive force on the fluid chamber 672 causing the pressure of the fluid in the interior region of the fluid chamber 672 to be increased. This increased pressure can be communicated through the fluid from the fluid chamber 672 to and through the conduit 676 and to the pressure transducer 649 via a conduit (not shown) connecting the conduit 676 to the pressure transducer 649 via the connector 673. The force sensor device 648 can be used to measure the load on a tether extending through the positioning device to which the force sensor device 648 is coupled.

[1121] For each of the embodiments of a positioning device described herein (242, 342, 442), in some cases, after deployment, the tether may be left having excess length, i.e. not trimmed, in order to facilitate later capture if necessary. If it is determined that the length of the tether is not suitable for some reason, e.g., regurgitation is seen post-procedure and the tether is too slack or the tension is too high and the apical tissue is invaginating or changing the shape of the heart in an unwanted manner, the positioning device can be used to capture the excess untrimmed tail of the tether, thread the tether through the positioning device, re-

engage the epicardial anchor device, unlocking the pin assembly of anchor device and allowing for the tether length adjustment. The tether may then be adjusted length-wise, either shorter or longer, and the tether is then re-tested for tensioning force, re-pinned and locked into place with the epicardial anchor device.

[1122] In some cases, tether tightening or shortening may be, for example, in the range from about 1mm-10mm, or about 1mm-8mm, or about 1mm-5mm, or about 2mm-8mm, or about 2mm-5mm in length, and all ranges inclusive. Tether loosening or lengthening is contemplated as ranging from about 1mm-10mm, or about 1mm-8mm, or about 1mm-5mm, or about 2mm-8mm, or about 2mm-5mm in length and all ranges inclusive.

[1123] It is contemplated that the time range for which post-deployment adjustments to the tether length or position can be, for example, from about 0.5 hours-48 hours, or from about 24 hours-72 hours, or from about 1 day-7 days, or from about 1 day-15 days, or from about 1 day-30 days, post-implantation.

[1124] In an alternative embodiment of a positioning device, a force sensor device can be included that includes a mechanical indicator. For example, a spring device may be connected to a mechanical tension meter to show load range. A load of 1-2 lbs. or 1-4 lbs. are examples of a typical target load.

[1125] Although not shown, an alternative to the vice type of tether securing device described herein (e.g., 247, 347), a pinning device that can be used. For example, such a device can include a portion through which the tether can be threaded, and a pin member can be operatively coupled thereto and actuated to pierce through the tether to hold the tether in position. Such a device can be incorporated into a positioning device and be operatively coupled to an actuation mechanism. In some embodiments, such a pinning mechanism can be manually actuated.

[1126] FIGS. 32-35 illustrate an alternate embodiment of a tether release tool that can be used for capturing a tether, and engaging/re-engaging an epicardial pad after it has been deployed. As shown, for example, in FIGS. 32 and 33, the tether release tool 580 includes a handle 581 coupled to an elongate positioning rod 582. The positioning rod 582 includes a shaped anchor engagement tip 583 and defines a tether capture/recapture access port 584. As shown in FIG. 33, the anchor engagement tip 583 is shaped to be received in a corresponding mating opening 510 of an epicardial anchor device 500 (see, FIGS. 34 and 35), which can be

configured the same and function the same as the epicardial anchor device 200 described above. The engagement tip 583 defines an opening 585 that is in fluid communication with the access port 584.

[1127] After the epicardial anchor device 500 has been deployed and the tether 528 has been pinned to the anchor device 500, the tether release tool 580 can be used to release the tether to allow the practitioner to make adjustments to the tension on the tether 528 and/or to the position of the anchor device 500. As shown in FIGS. 34 and 35, a portion of the tether 528 extending from the anchor device 528 is inserted through the distal opening 585 and out through the access port 584. The engagement tip 583 can be inserted into the mating opening 510 of the anchor device 500. The tether release tool 580 can be rotated to unlock the locking assembly of the anchor device 500 to release the tether 528 from the anchor device 500. With the tether 528 released, the tension on the tether can be adjusted and/or the position of the anchor device 500 on the heart can be adjusted and then the tether release tool 580 can be used to re-pin the tether 528 to the anchor device. For example, the engagement tip 583 can be inserted into the mating opening 510 of the anchor device 500 and rotated the opposite direction to re-actuate the locking pin assembly of the anchor device 500 and pin the tether 528 to the anchor device 500.

[1128] In some embodiments, there is a tether-bundle that attaches to the extended points (two or three or four) of the stent and which converge to a central nexus point to which the adjustable tether is attached and leads to the apical tissue anchor location within the heart. In some embodiments, the tether extends downward through the left ventricle, exiting the left ventricle at the apex of the heart to be fastened on the epicardial surface outside of the heart. Similar anchoring is contemplated herein as it regards the tricuspid, or other valve structure requiring a prosthetic.

[1129] As described herein, during deployment of a prosthetic heart valve, the operator is able to adjust or customize the tethers to the correct length for a particular patient's anatomy. The tethers also allow the operator to tighten the cuff onto the tissue around the valvular annulus by pulling the tethers, which creates a leak-free seal. In some embodiments, the tethers are optionally anchored to other tissue locations depending on the particular application of the prosthetic heart valve. In the case of a mitral valve, or the tricuspid valve, there are optionally one or more tethers anchored to one or both papillary muscles, septum, and/or ventricular wall.

[1130] The tethers, in conjunction with the cuff of the valve, provide for a compliant valve which has heretofore not been available. The tethers can be made from surgical-grade materials such as biocompatible polymer suture material. Examples of such material include 2-0 ePTFE (polytetrafluoroethylene) or 2-0 polypropylene. In one embodiment, the tethers are inelastic. It is also contemplated that one or more of the tethers may optionally be elastic to provide an even further degree of compliance of the valve during the cardiac cycle. In some embodiments the tether(s) may be bioresorbable/bioabsorbable and thereby provide temporary fixation until other types of fixation take hold such as a biological fibrous adhesion between the tissues and prosthesis and/or radial compression from a reduction in the degree of heart chamber dilation.

[1131] While various embodiments have been described above, it should be understood that they have been presented by way of example only, and not limitation. Where methods described above indicate certain events occurring in certain order, the ordering of certain events may be modified. Additionally, certain of the events may be performed concurrently in a parallel process when possible, as well as performed sequentially as described above.

[1132] Where schematics and/or embodiments described above indicate certain components arranged in certain orientations or positions, the arrangement of components may be modified. While the embodiments have been particularly shown and described, it will be understood that various changes in form and details may be made. Any portion of the apparatus and/or methods described herein may be combined in any combination, except mutually exclusive combinations. The embodiments described herein can include various combinations and/or sub-combinations of the functions, components, and/or features of the different embodiments described. For example, although not necessarily described for each embodiment, the various positioning devices (242, 342, 442) can include any features and/or functions described herein for the various embodiments.

What is claimed is:

1. An apparatus, comprising:
 - a handle assembly coupled to an elongate member;
 - a docking member coupled to a distal end of the elongate member, the docking member including a plurality of arms configured to be releasably coupled to an epicardial anchor device configured to secure a tether extending from a prosthetic heart valve implanted within a heart at a location on an exterior of a ventricular wall of the heart; and
 - a force sensor device coupled to the handle assembly, the force sensor device configured to measure a force exerted on the force sensor device, the force associated with a tension of the tether extending through the elongate member and handle assembly, wherein the force sensor device includes a sensor housing, a fluid chamber disposed within the sensor housing and a load washer coupled to the sensor housing such that the fluid chamber is disposed between the sensor housing and the load washer, the fluid chamber containing a volume of fluid, the volume of fluid being displaced when the force is exerted on the force sensor device.

2. The apparatus of claim 1, further comprising:
 - a tether securing device coupled to the handle assembly proximal to the force sensor device, the tether securing device configured to secure the tether extending through the elongate member and handle assembly at a fixed position relative to the handle assembly.

3. The apparatus of claim 1, further comprising:
 - a tether securing device coupled to the handle assembly proximal to the force sensor device, the tether securing device configured to secure the tether extending through the elongate member and handle assembly at a fixed position relative to the handle assembly, the tether securing device configured to contact the force sensor device and exert the force on the force sensor device as the tether is pulled proximally to a desired tension.

4. The apparatus of claim 1, further comprising:

a rod member coupled to the handle assembly; and

a tension member coupled to the rod member, the tension member configured to be moved distally relative to the rod member to adjust the tension on the tether extending through the elongate member and handle assembly.

5. The apparatus of claim 1, further comprising:

a rod member coupled to the handle assembly; and

a tension member coupled to the rod member, the rod member configured to be moved proximally when the tension member is rotated to adjust the tension on the tether extending through the elongate member and handle assembly.

6. The apparatus of claim 1, further comprising:

a rod member coupled to the handle assembly, the rod member having an indicator disposed at a distal end of the rod member, the handle assembly including a transparent segment with indications, the indicator disposed at the distal end of the rod member being viewable through the transparent segment, the tether extending through the apparatus having a marker disposed thereon, a location of the indicator relative to the indications on the transparent segment corresponding to a distance between a surface of the epicardial anchor device contacting the heart and an annulus of the heart when the marker on the tether is disposed proximal to a proximal end of the apparatus.

7. The apparatus of claim 1, wherein the handle assembly further comprises a dial, and the docking member further comprises a distal tip operably coupled to the distal end of the elongate member and configured to be received within the anchor device.

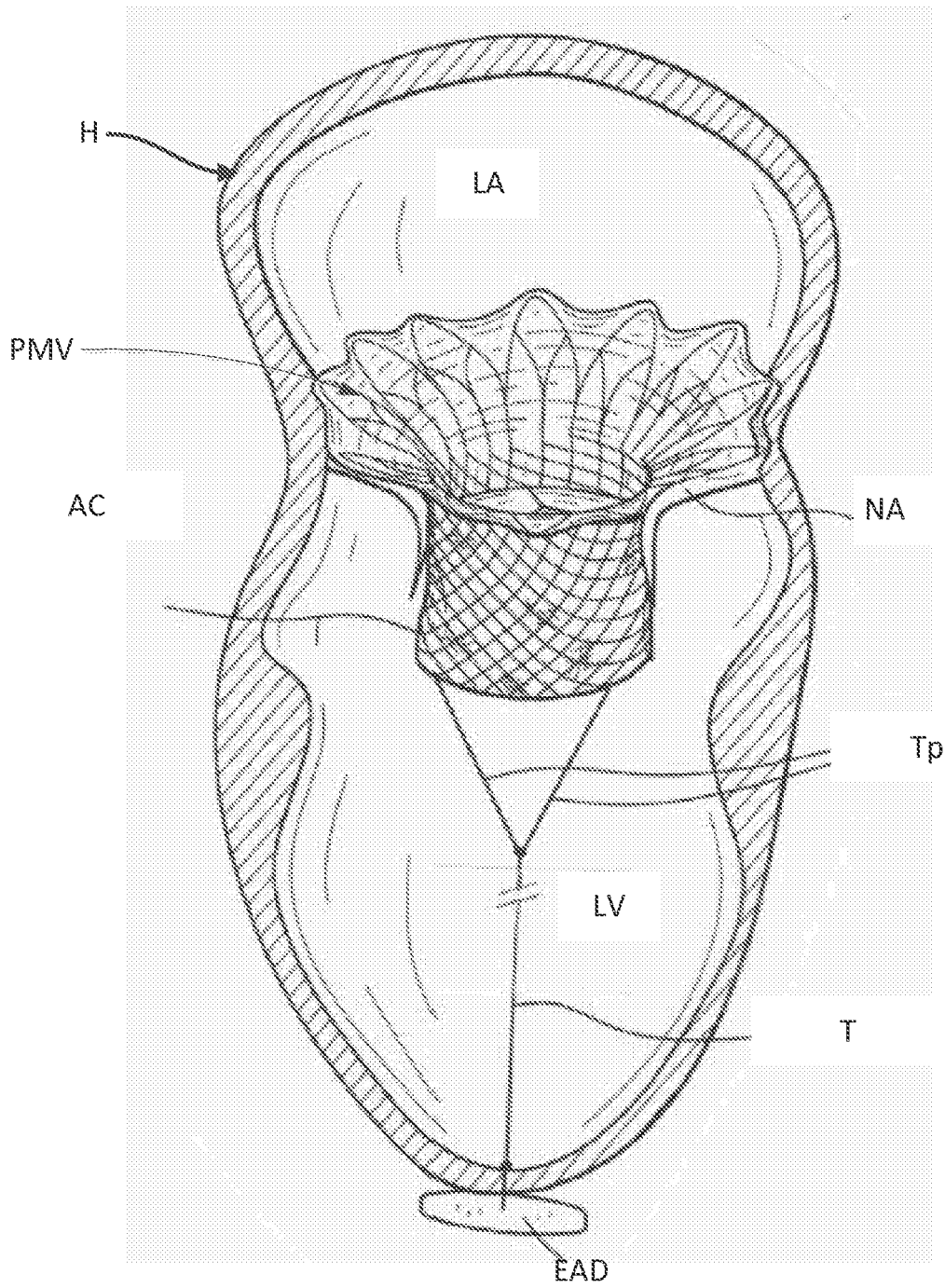


FIG. 1

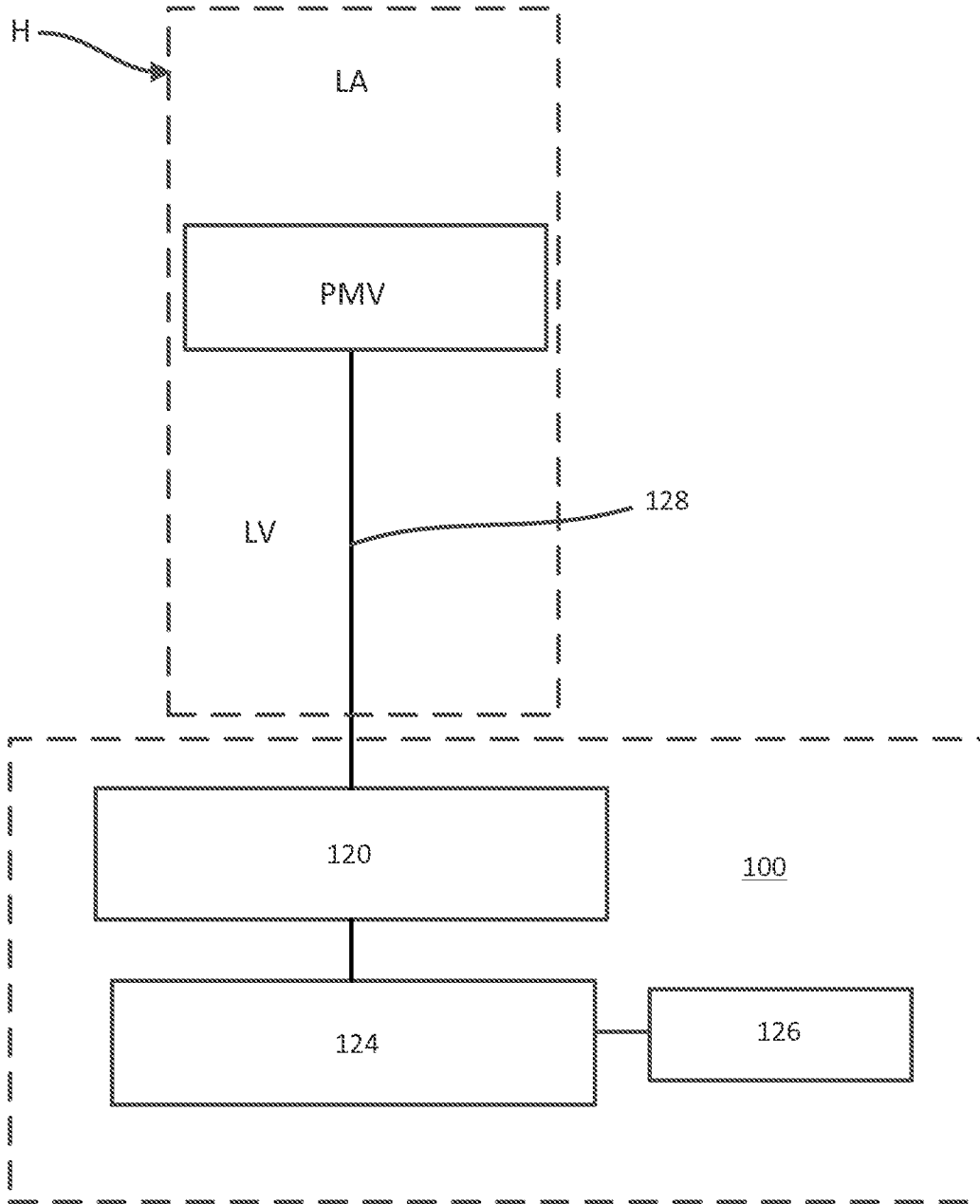


FIG. 2

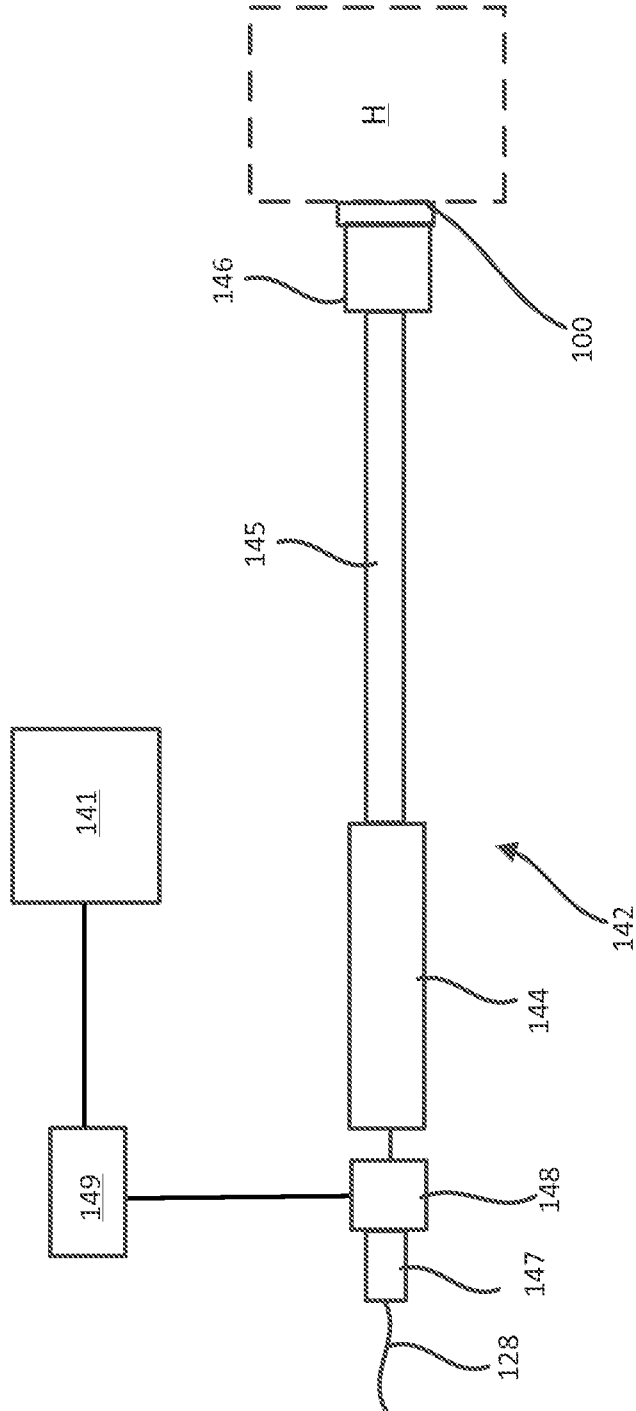


FIG. 3

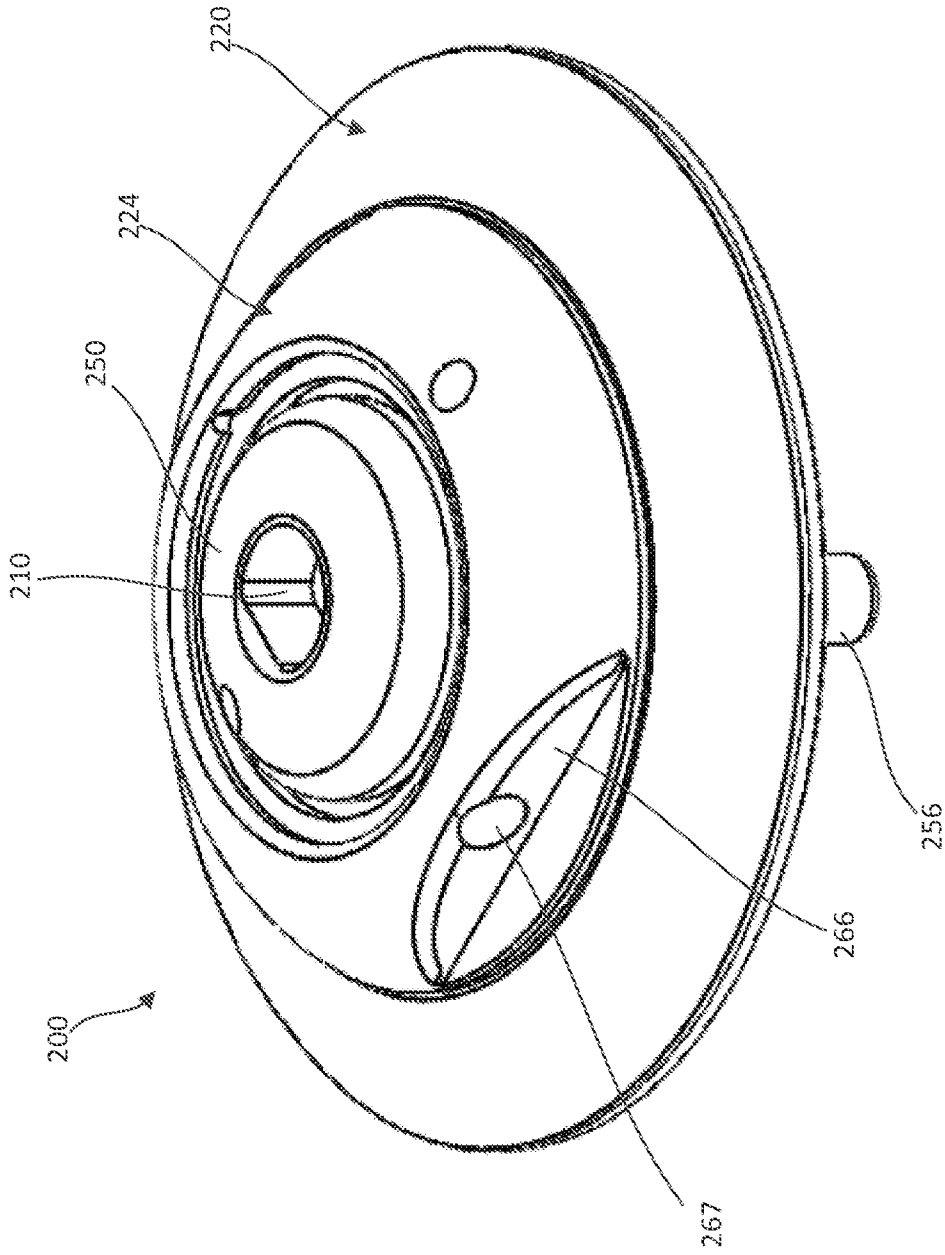


Fig. 4

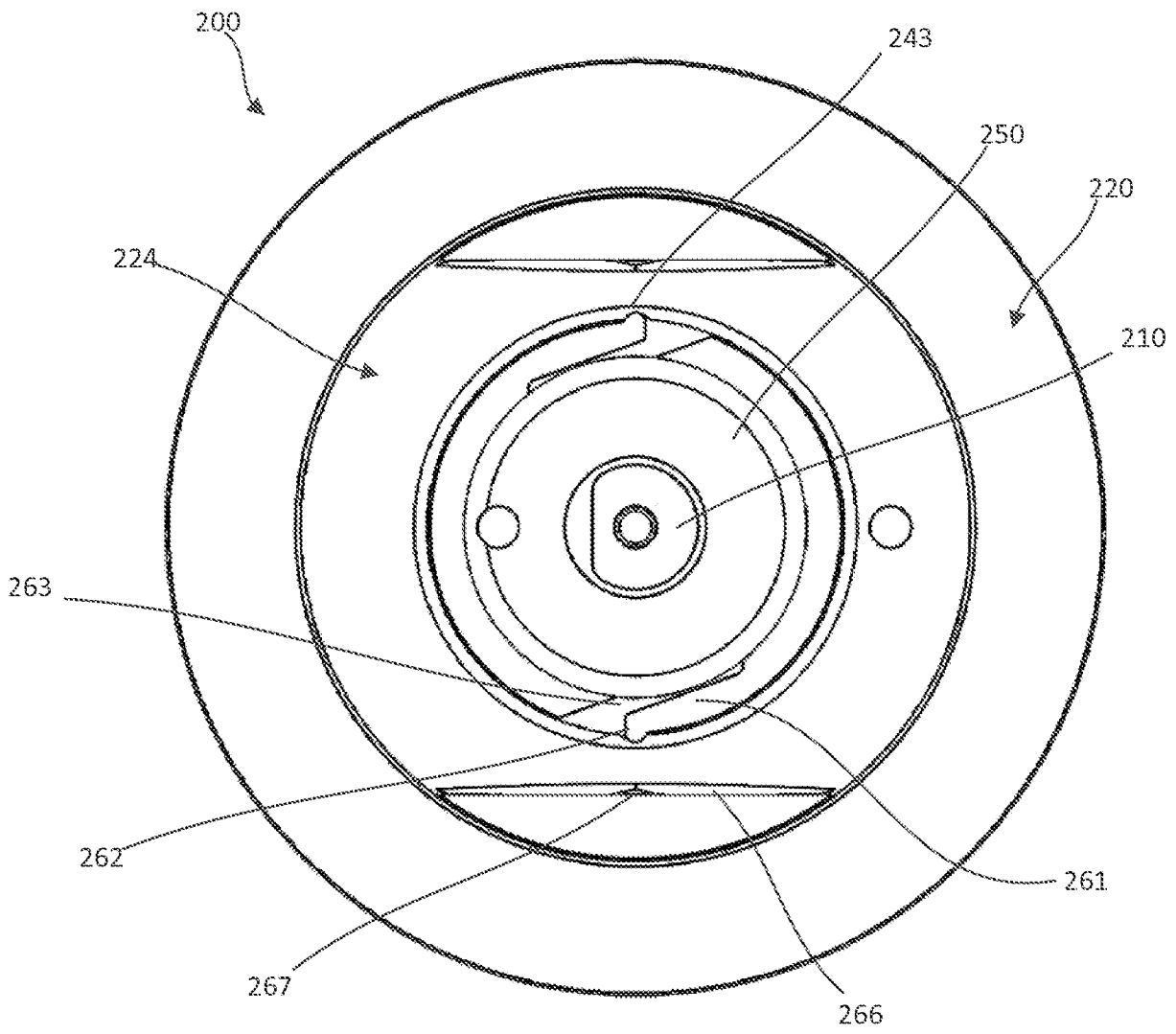


Fig. 5

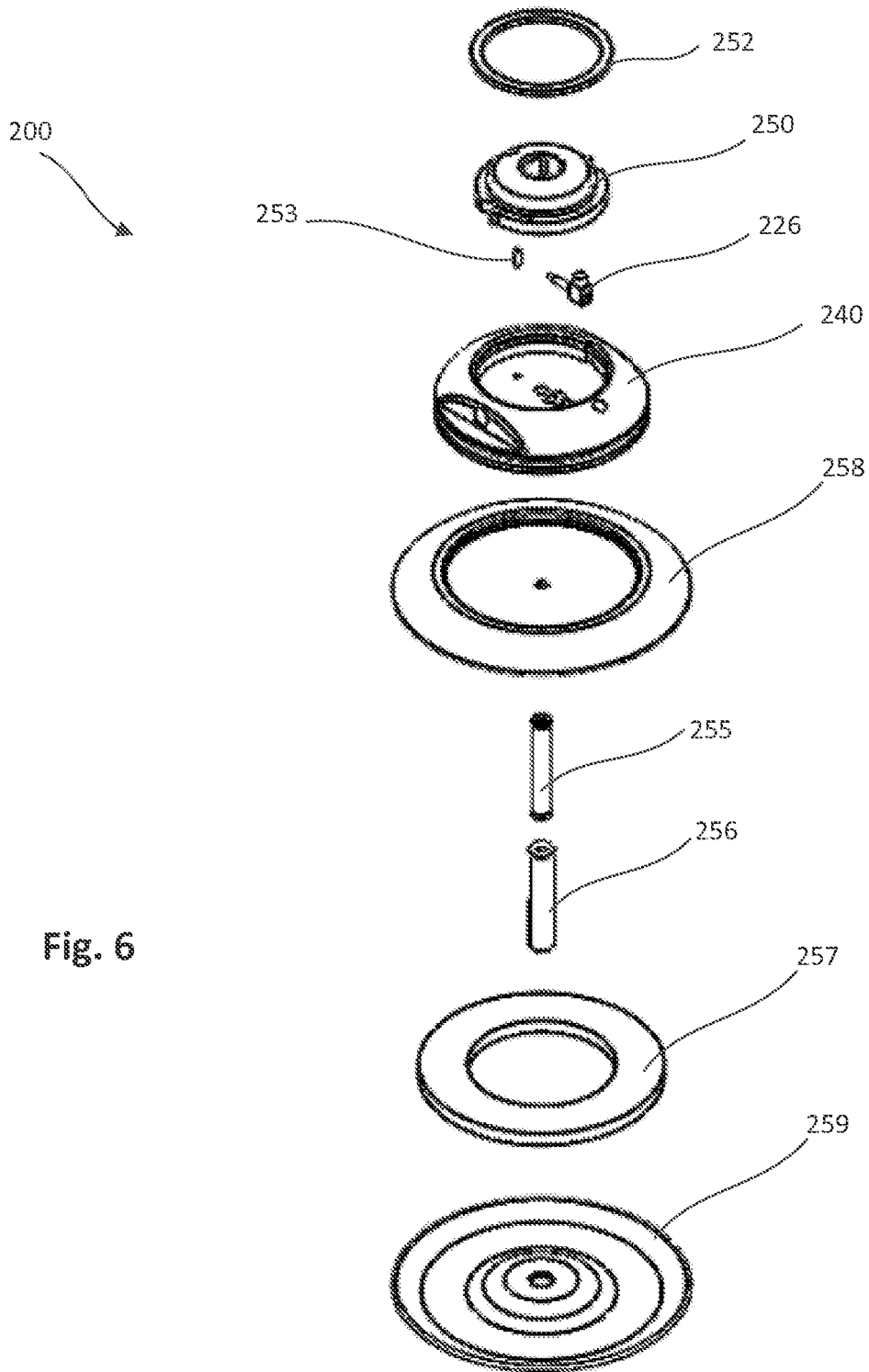


Fig. 6

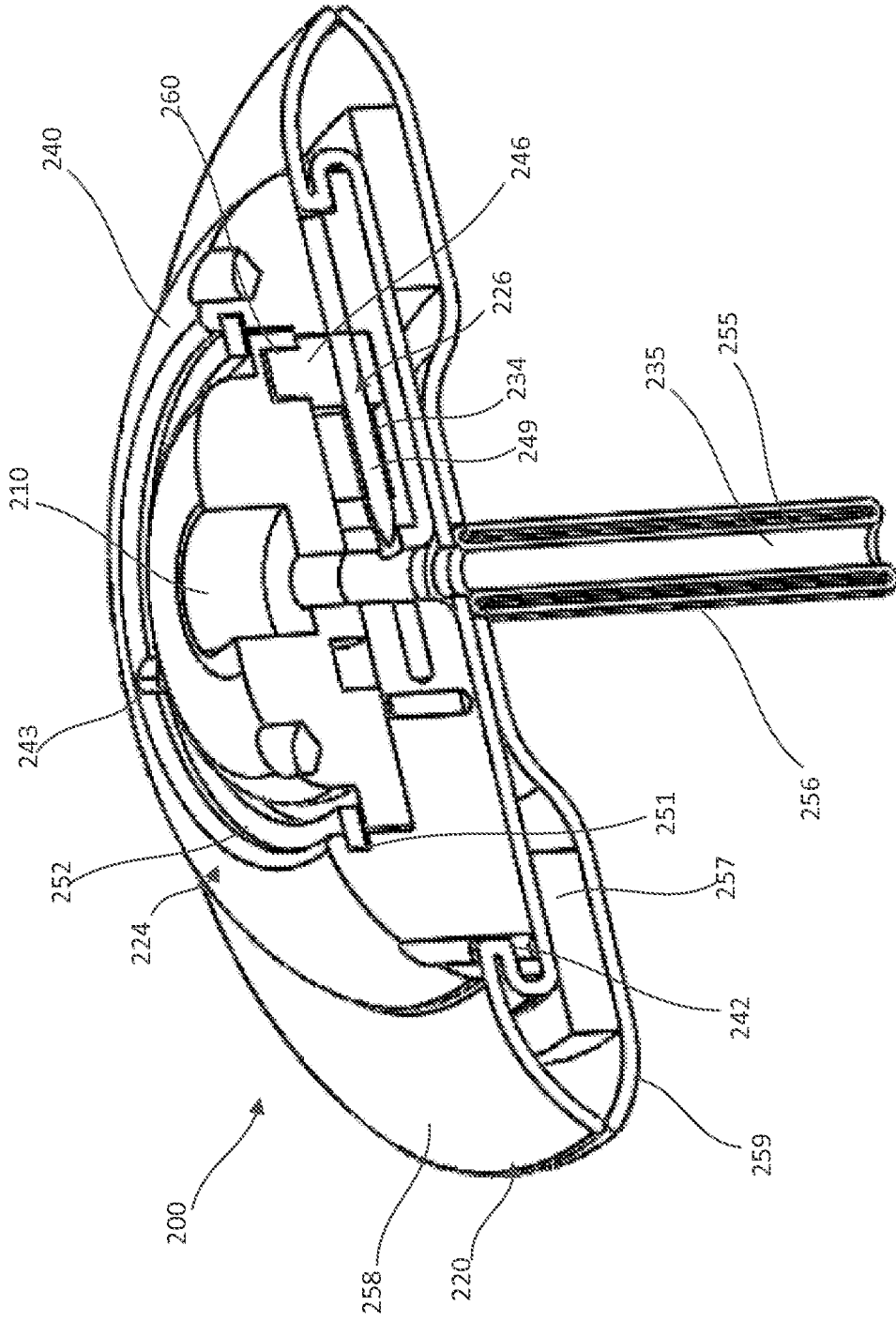


Fig. 7

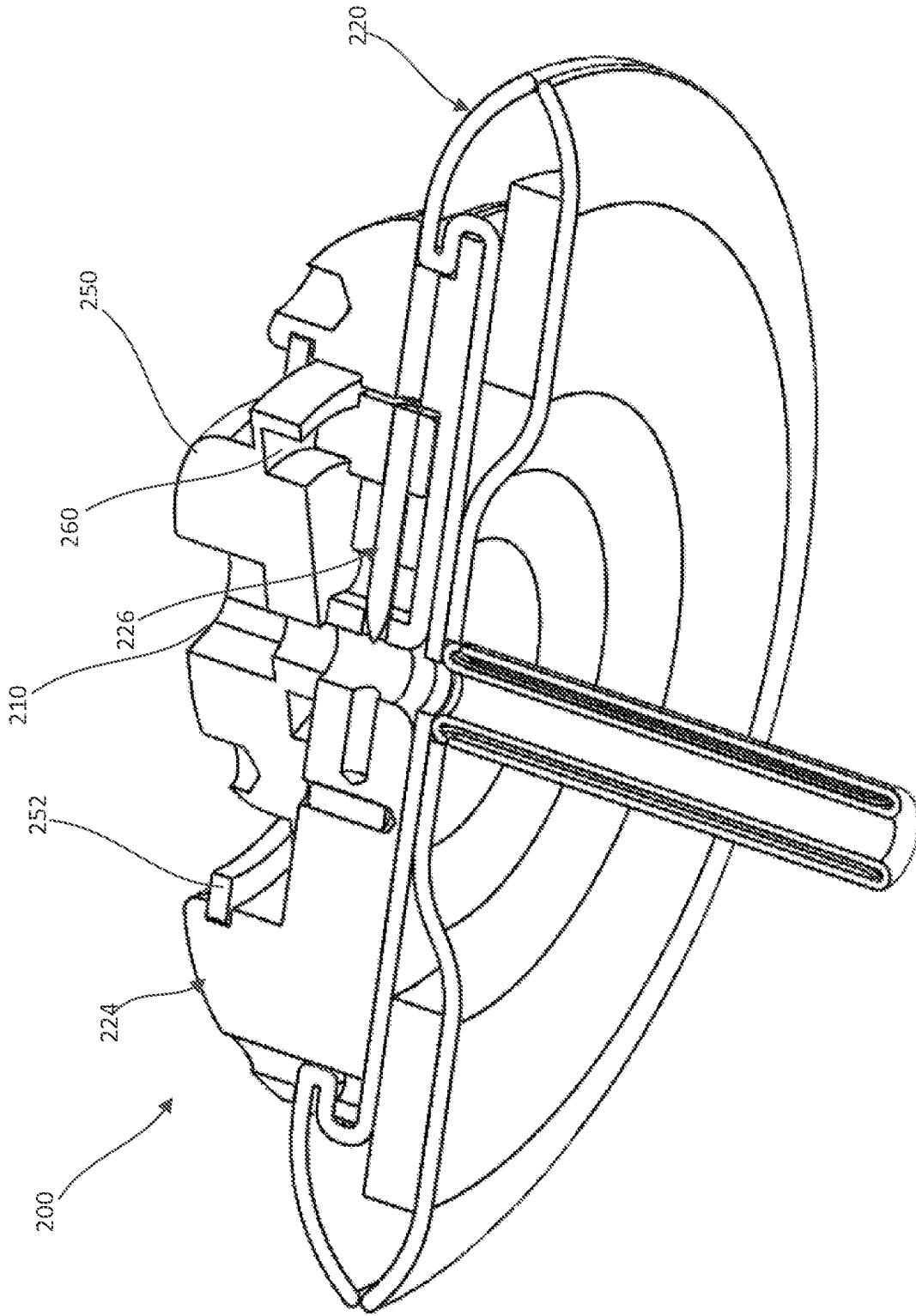


Fig. 9

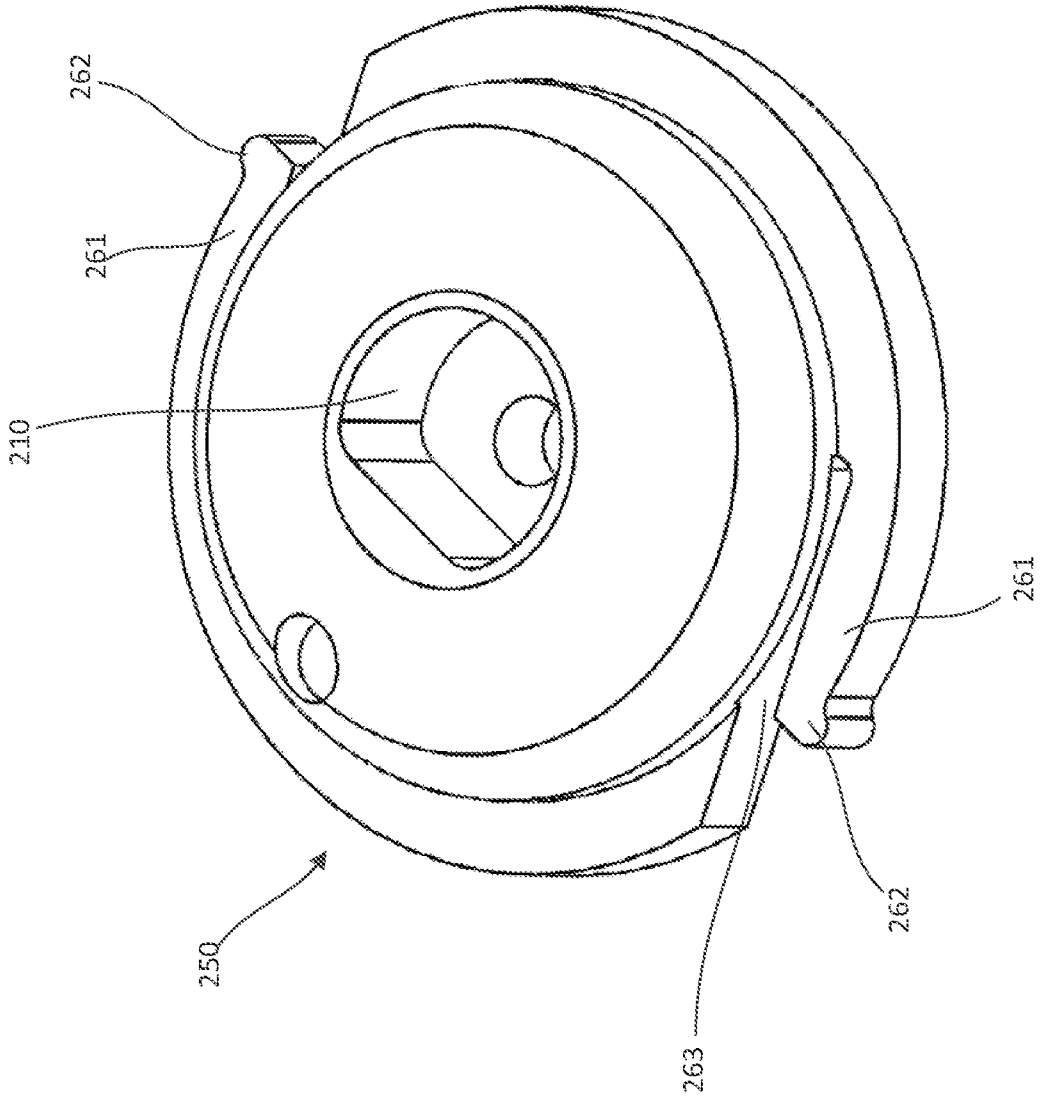


Fig. 10

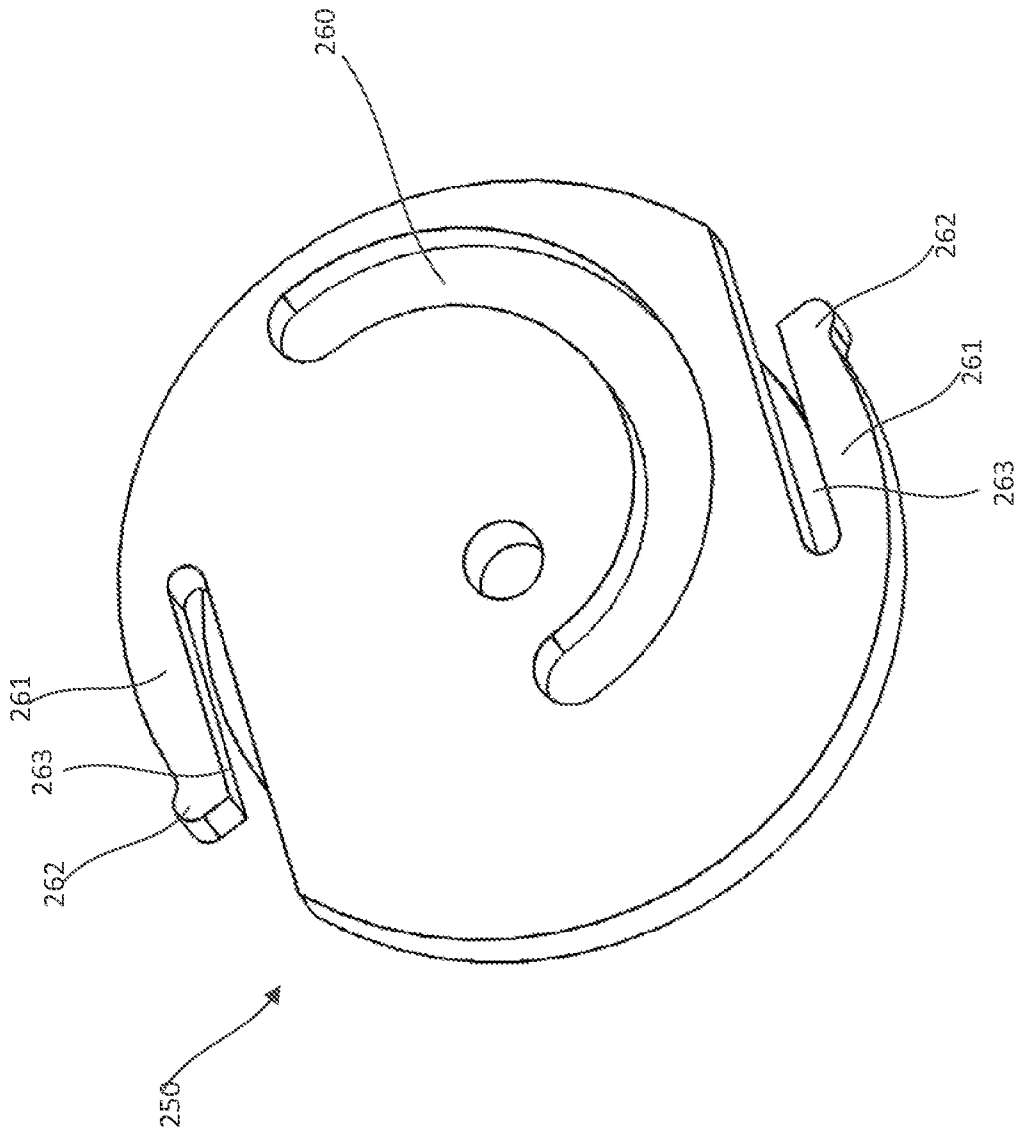


Fig. 11

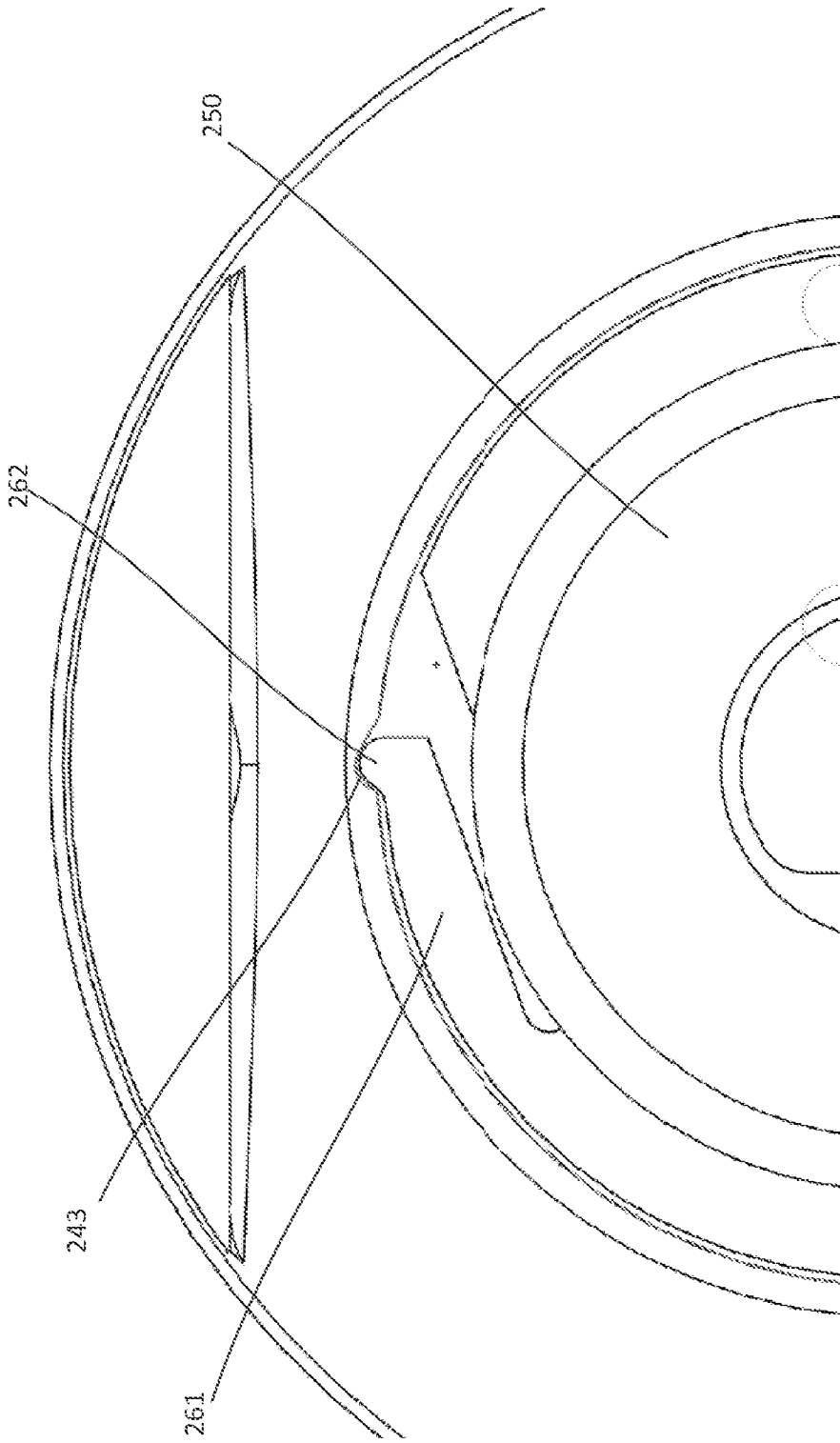


Fig. 12

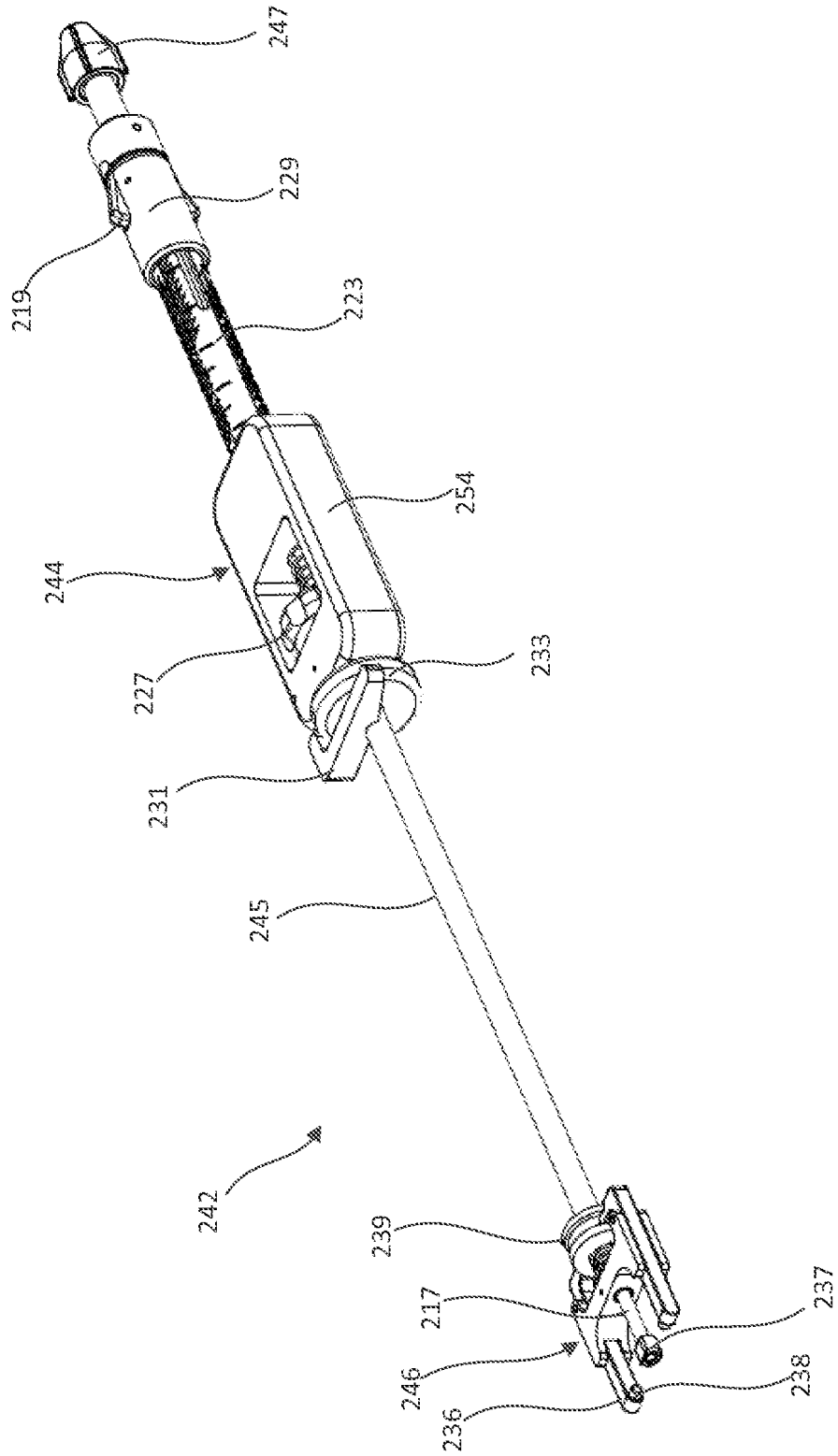


Fig. 13

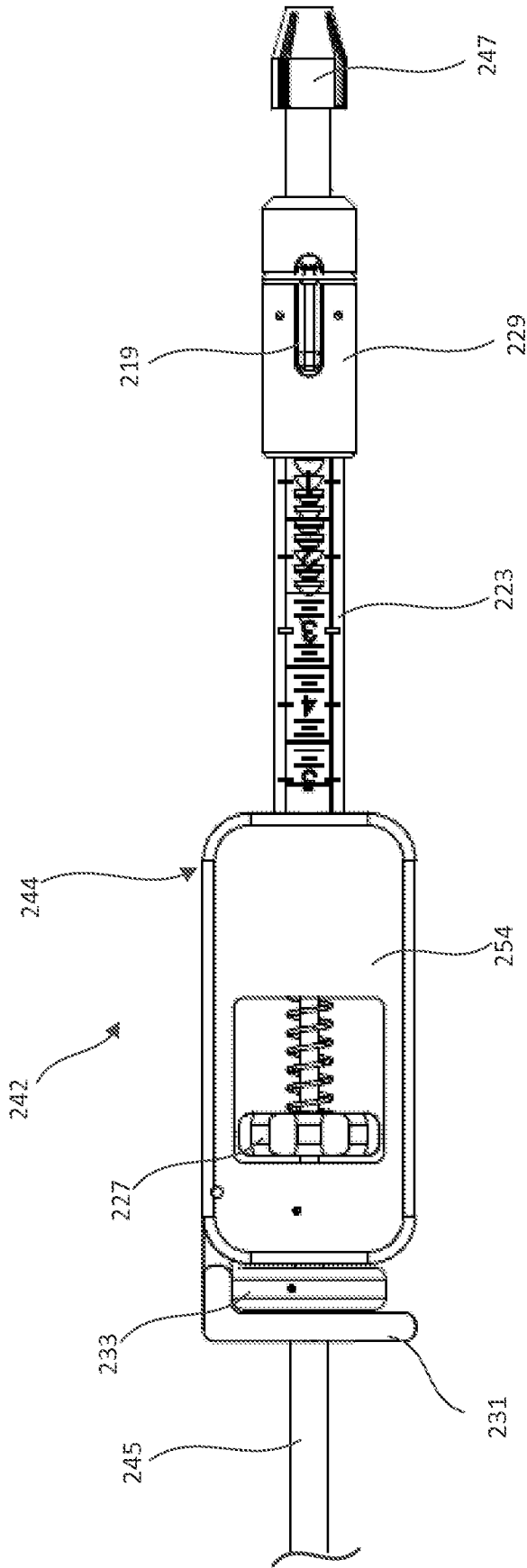


Fig. 14

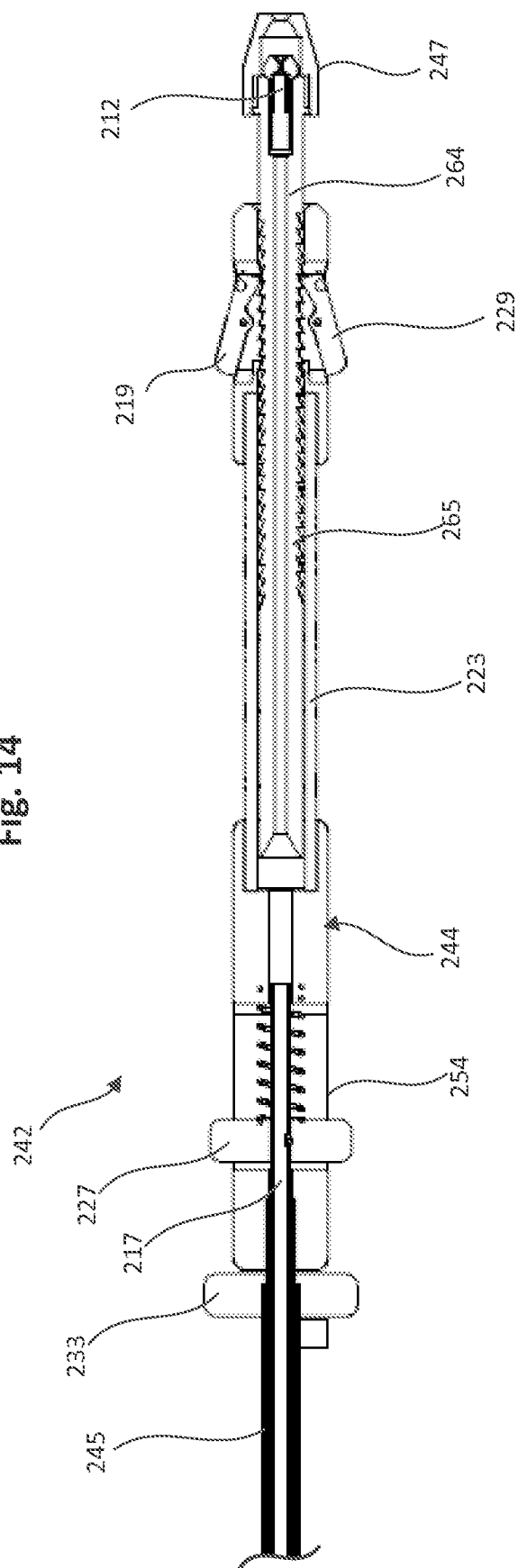


Fig. 15

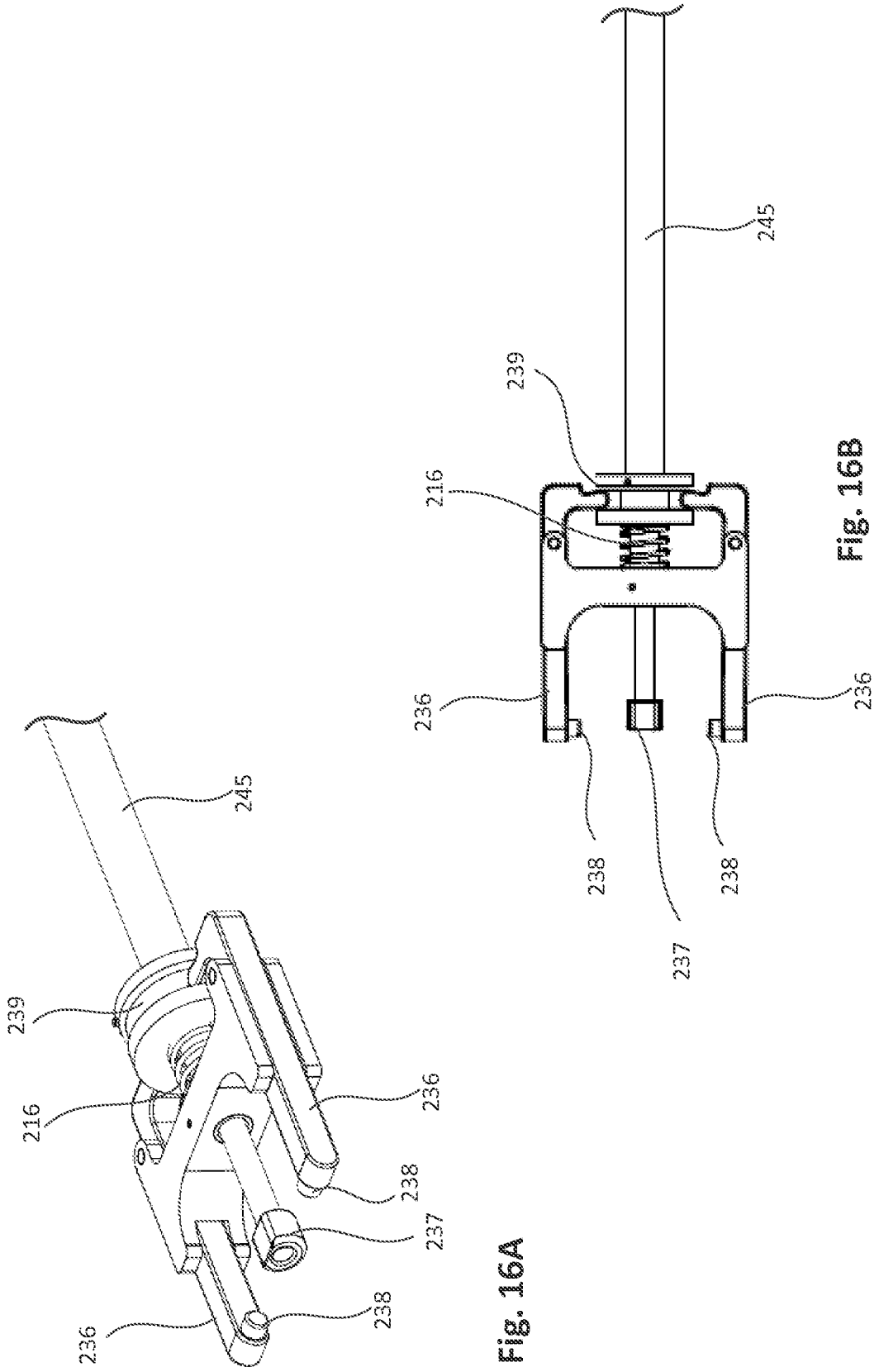


Fig. 16A

Fig. 16B

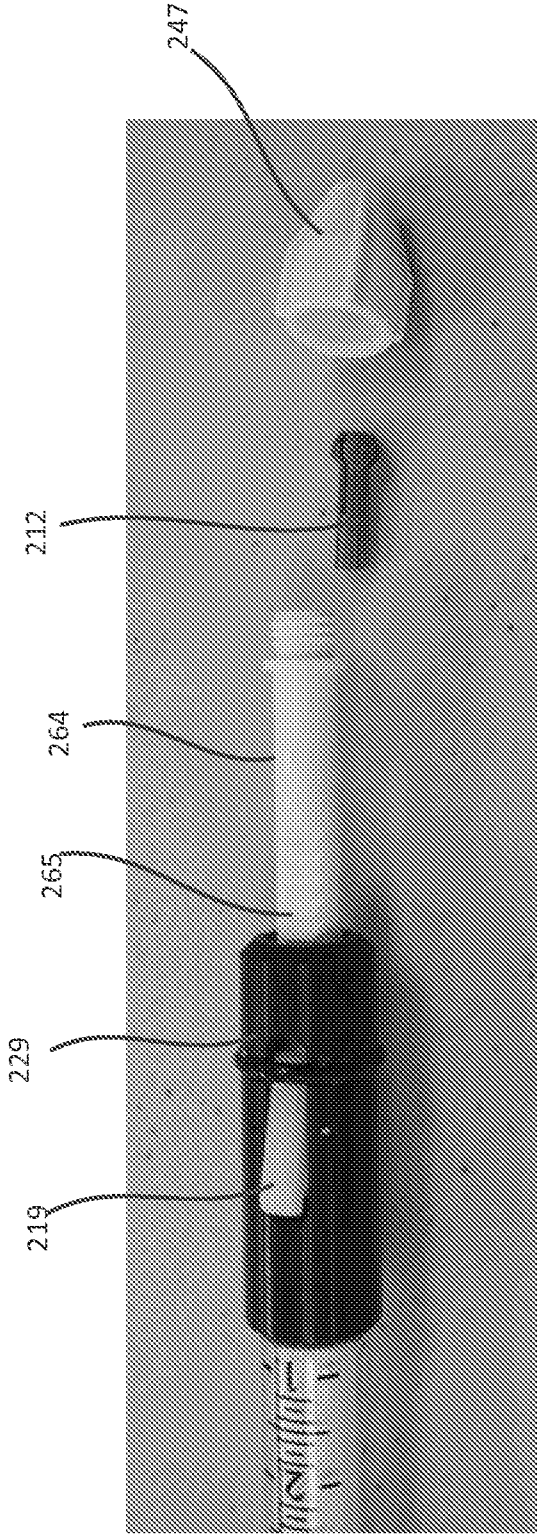


Fig. 17A

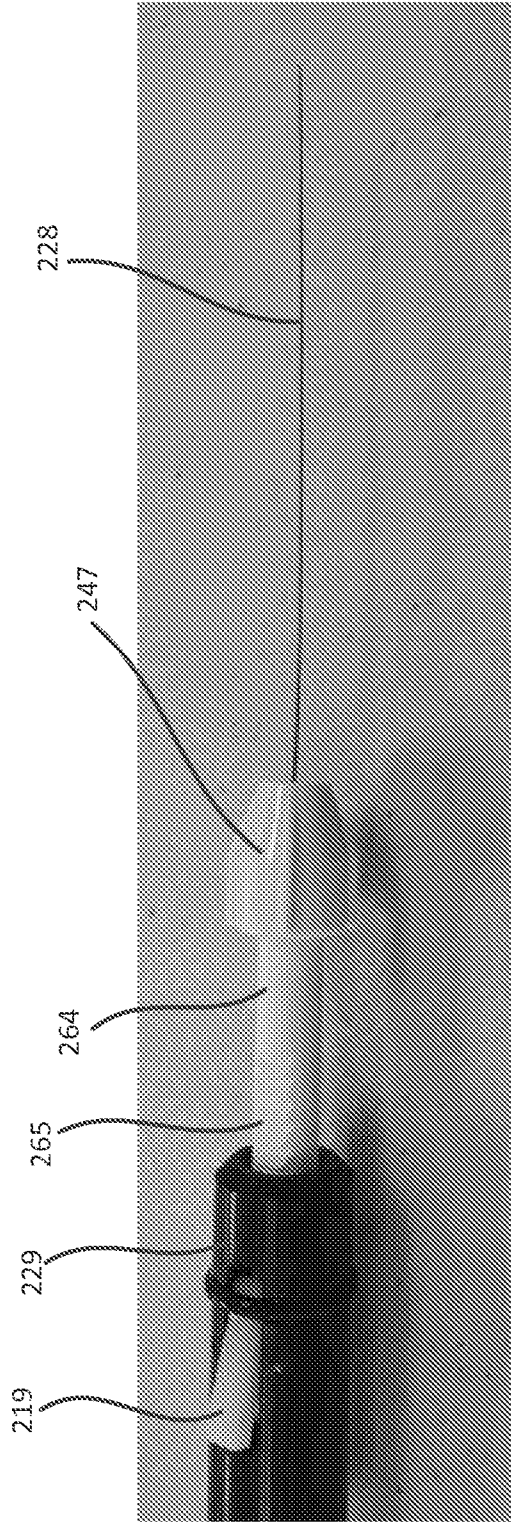


Fig. 17B

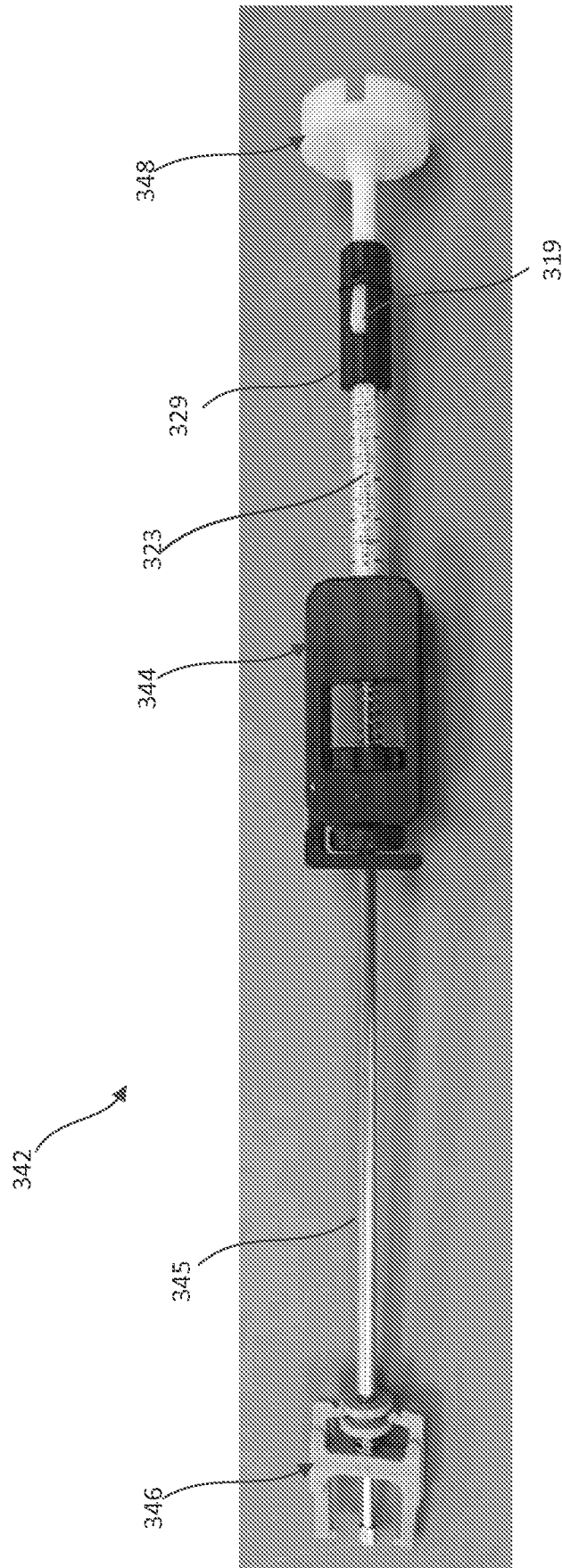


Fig. 18

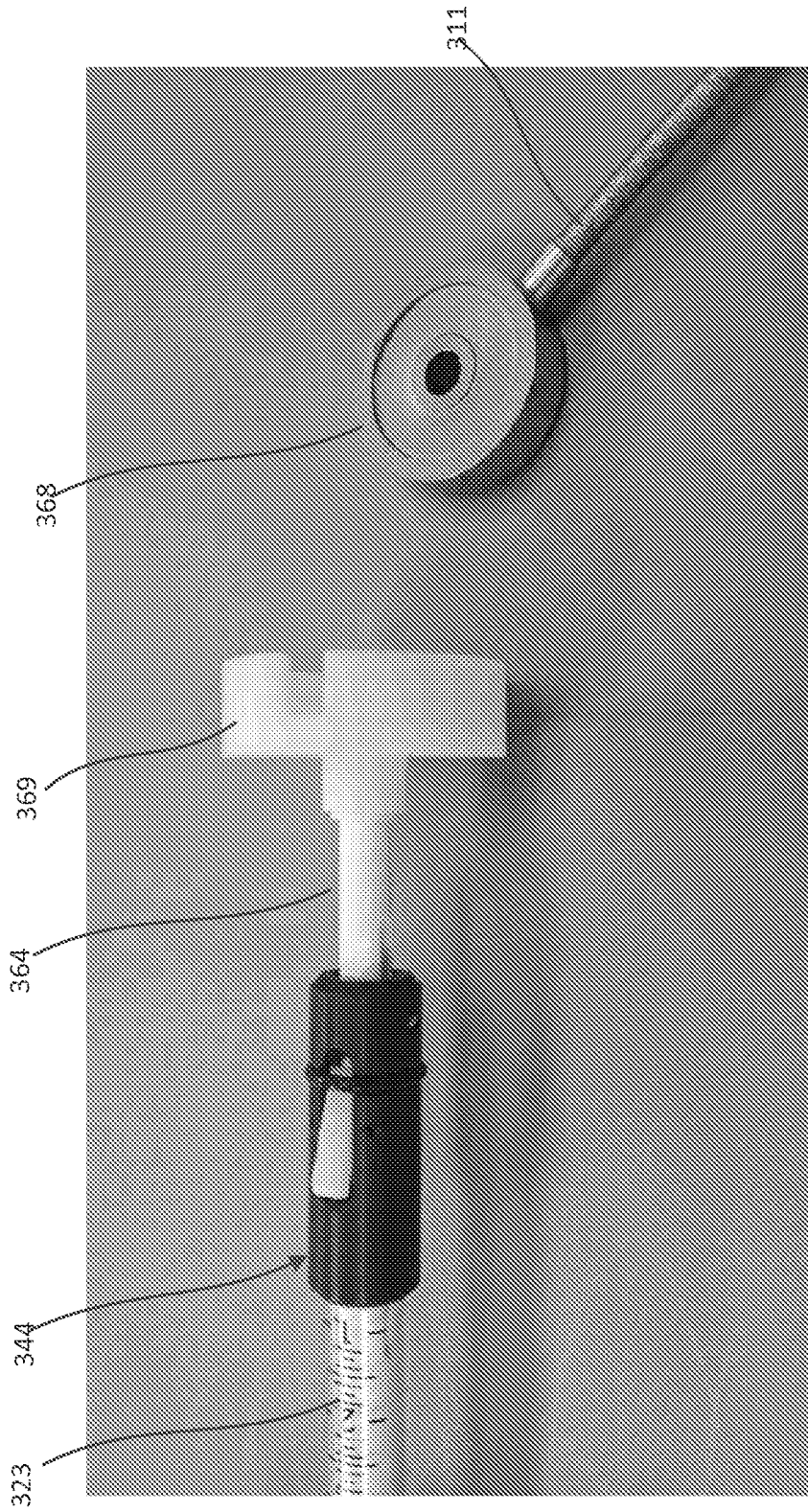


Fig. 19

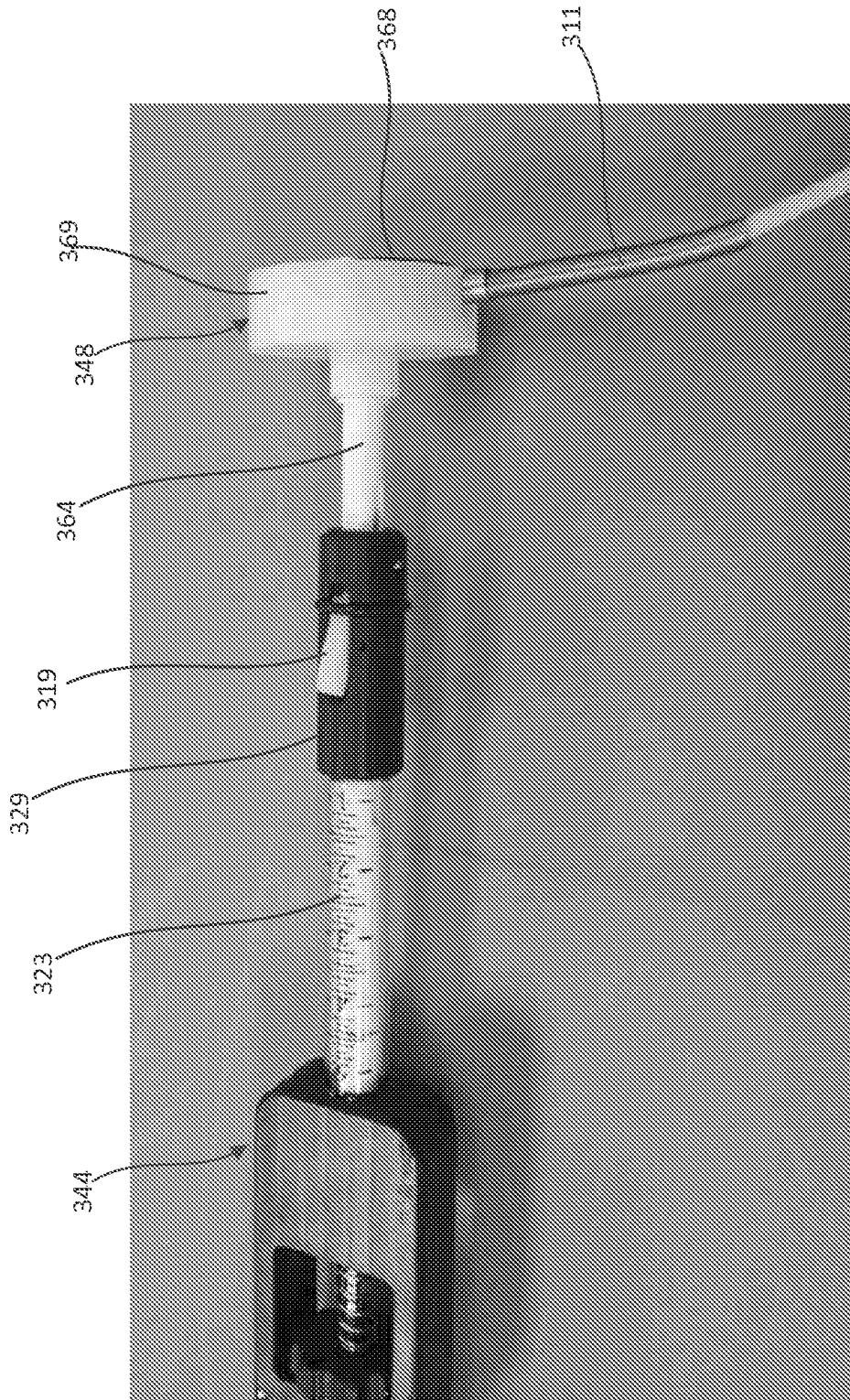


Fig. 20

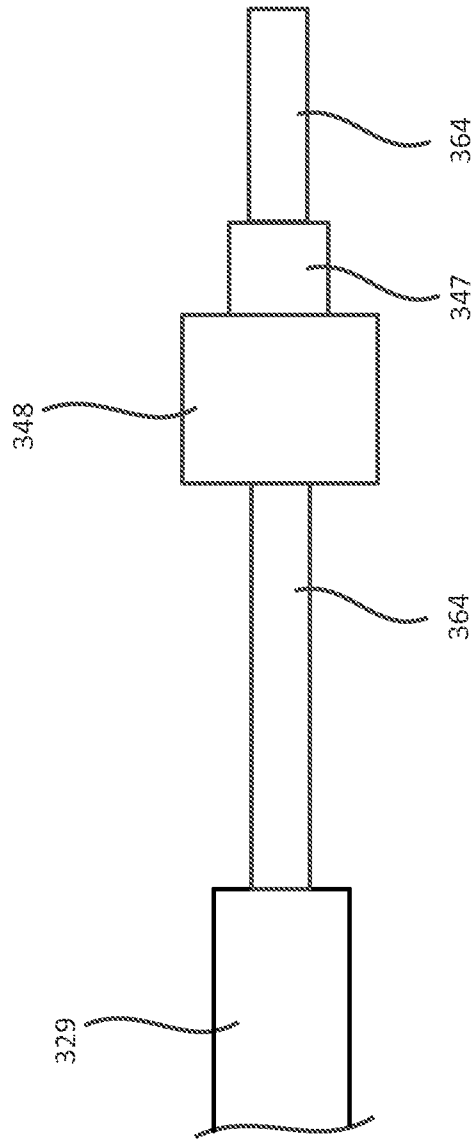


FIG. 21

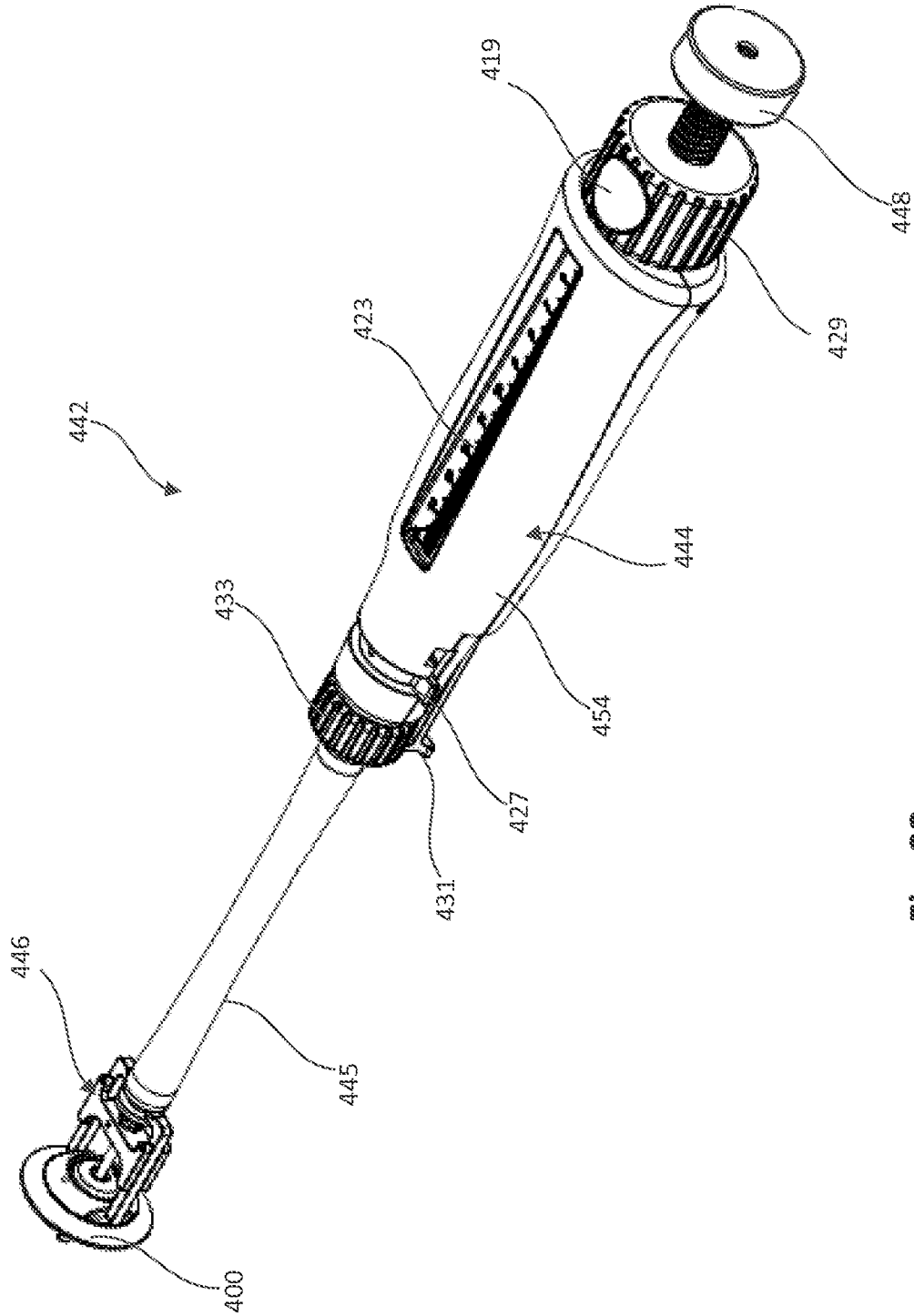


FIG. 22

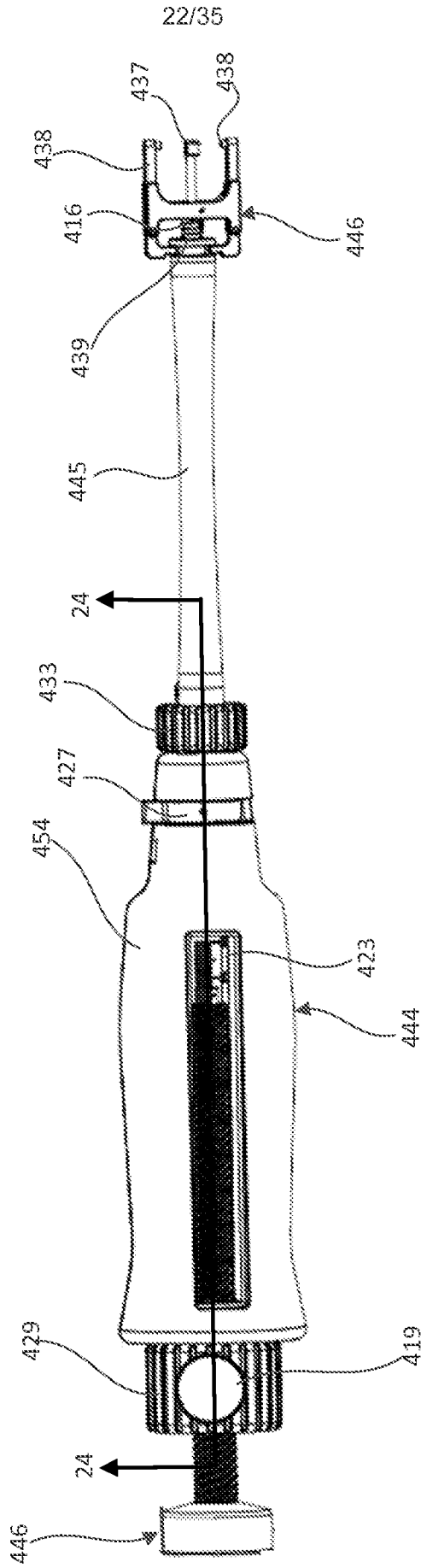


Fig. 23

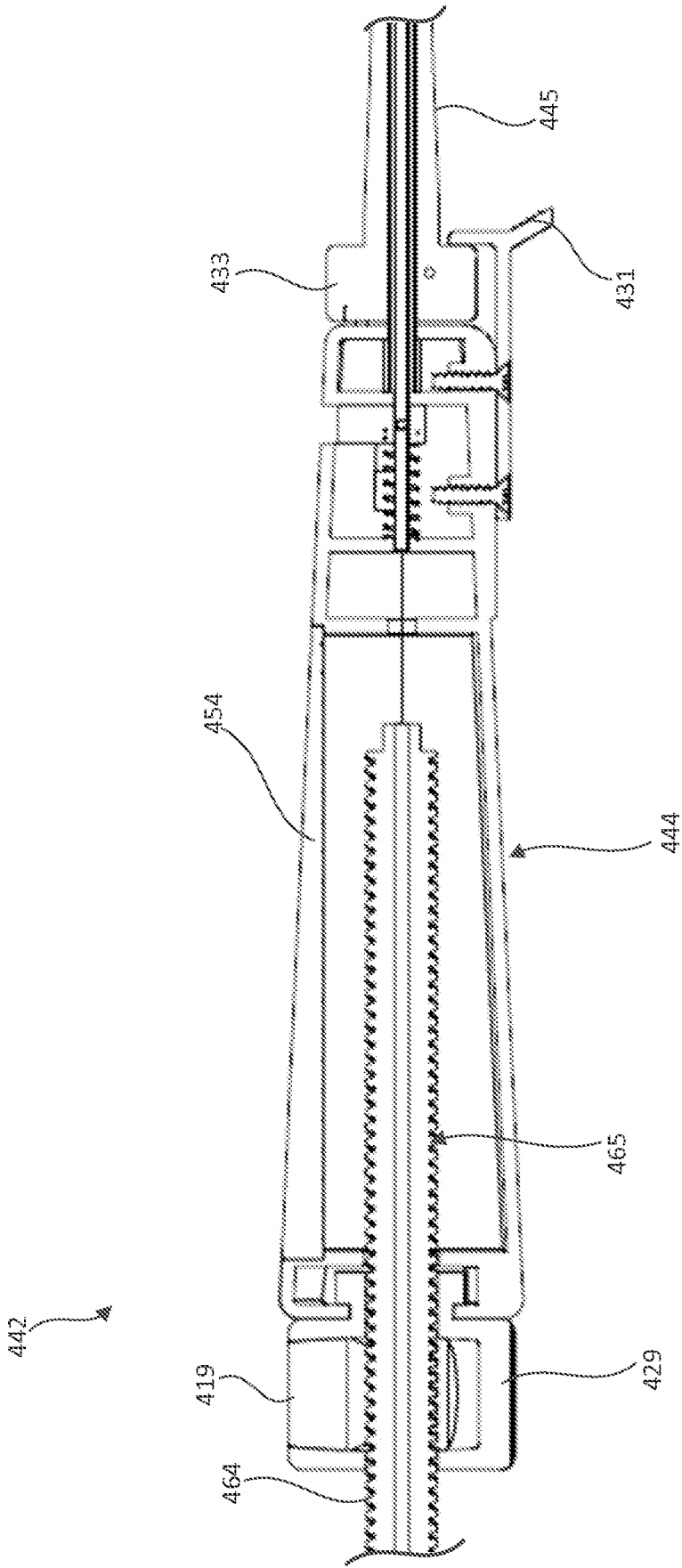


Fig. 24

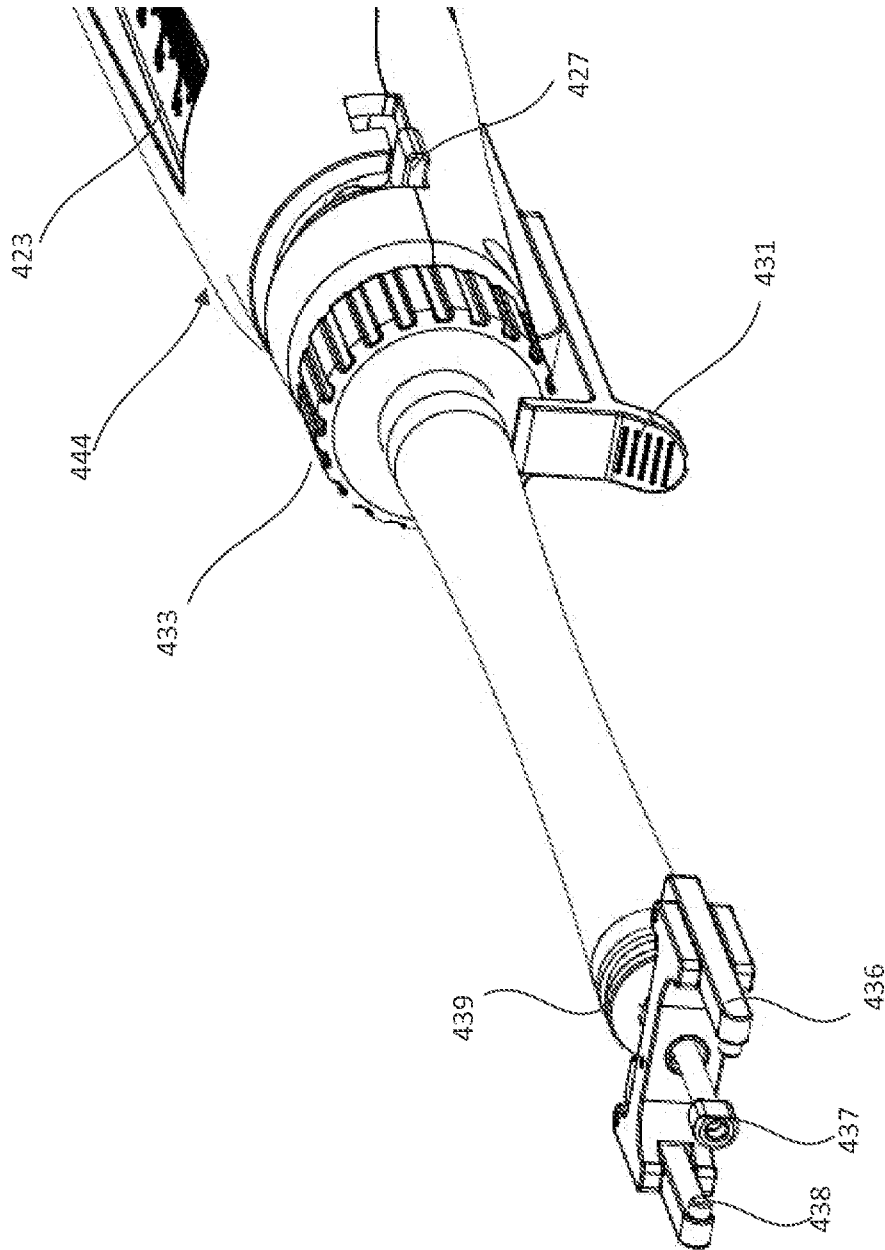


Fig. 25

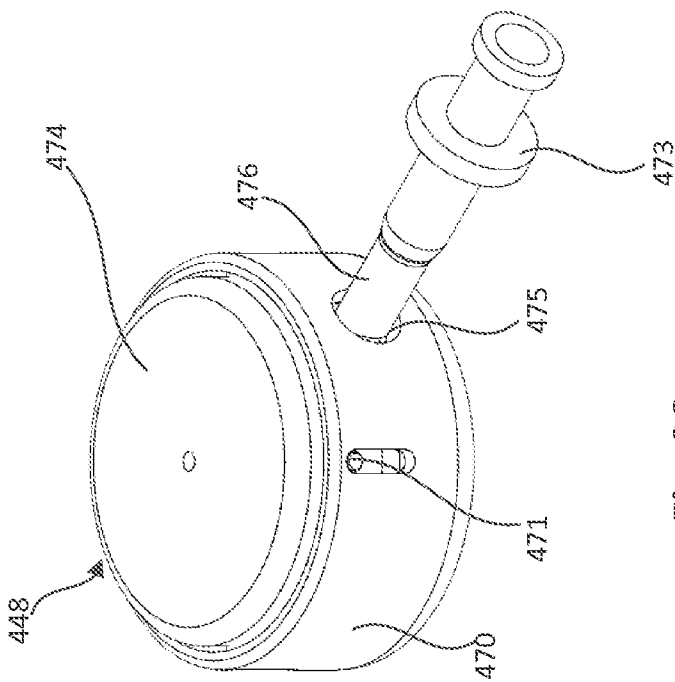


Fig. 26

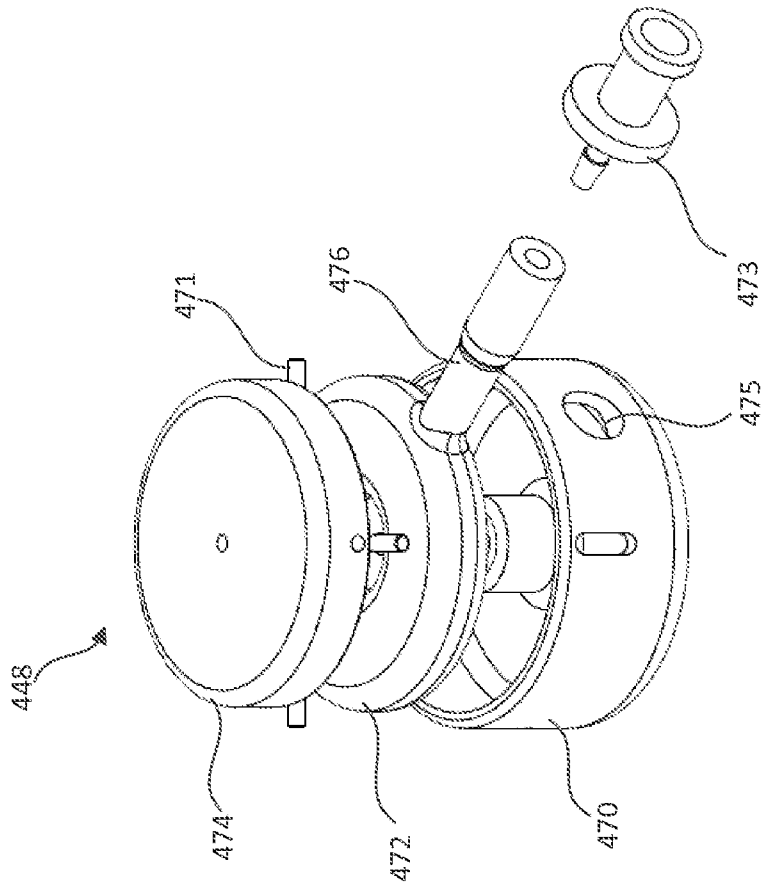


Fig. 27

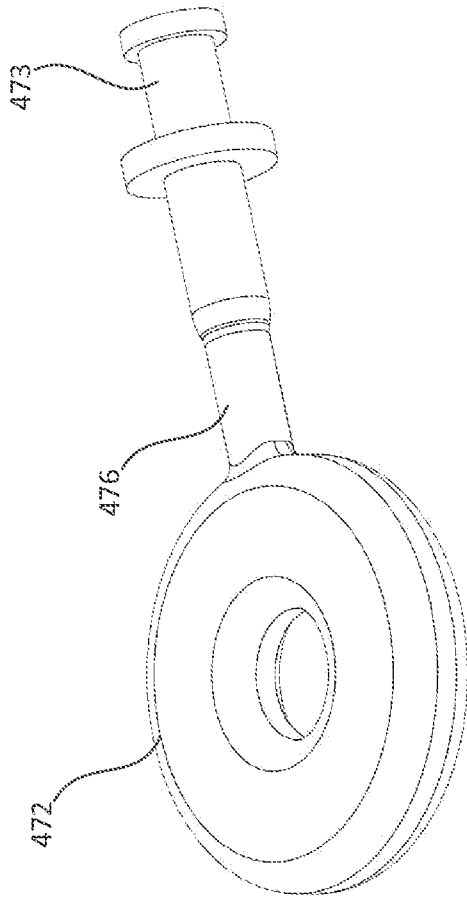


FIG. 28

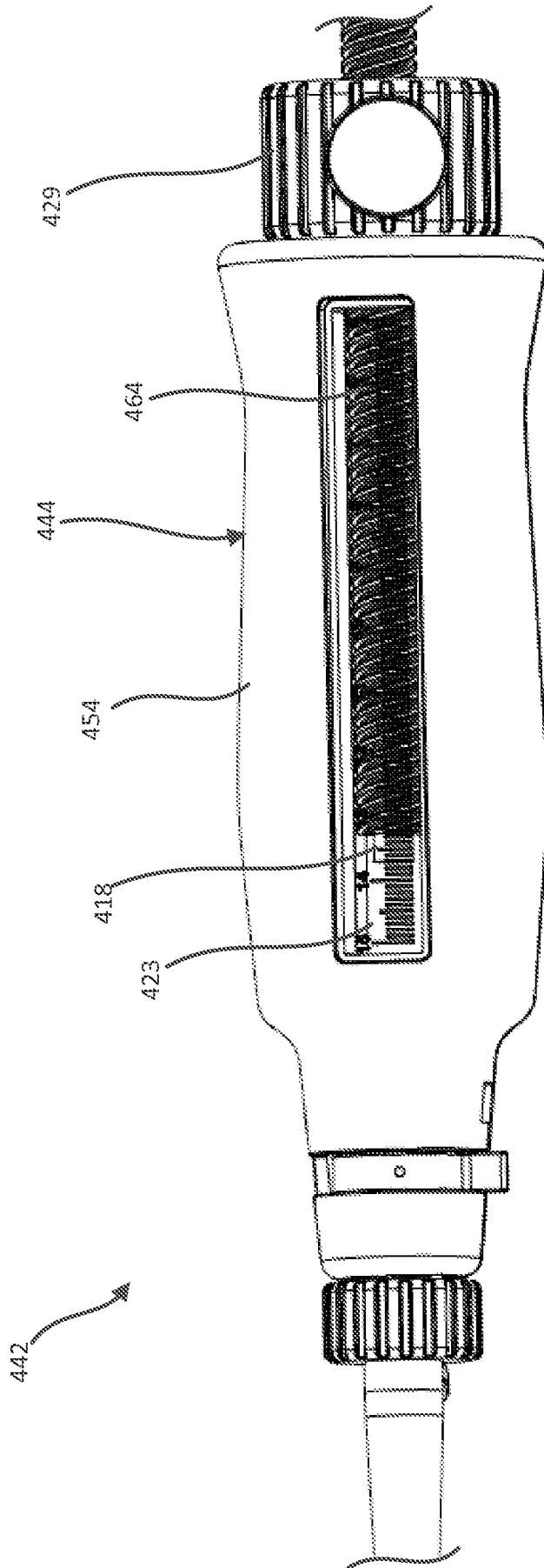


Fig. 29

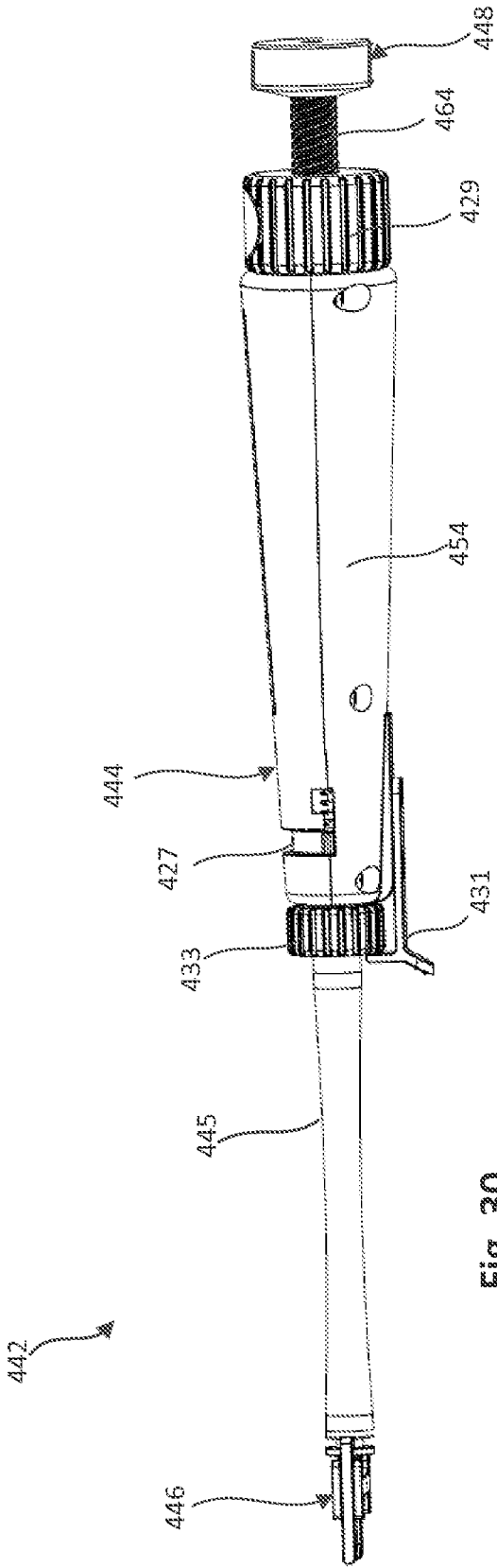


Fig. 30

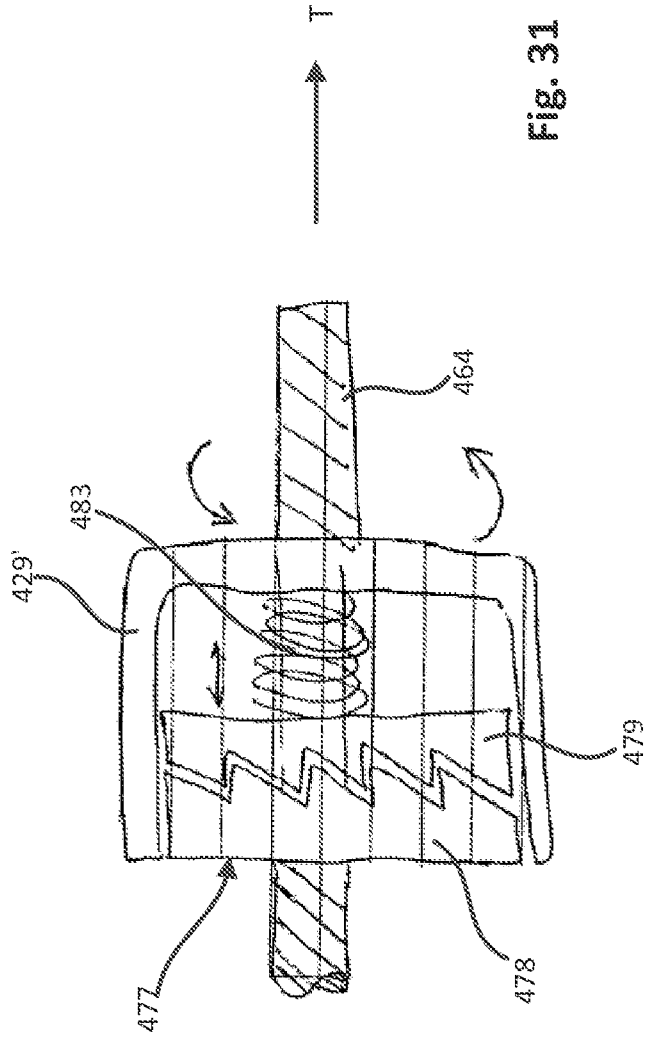


Fig. 31

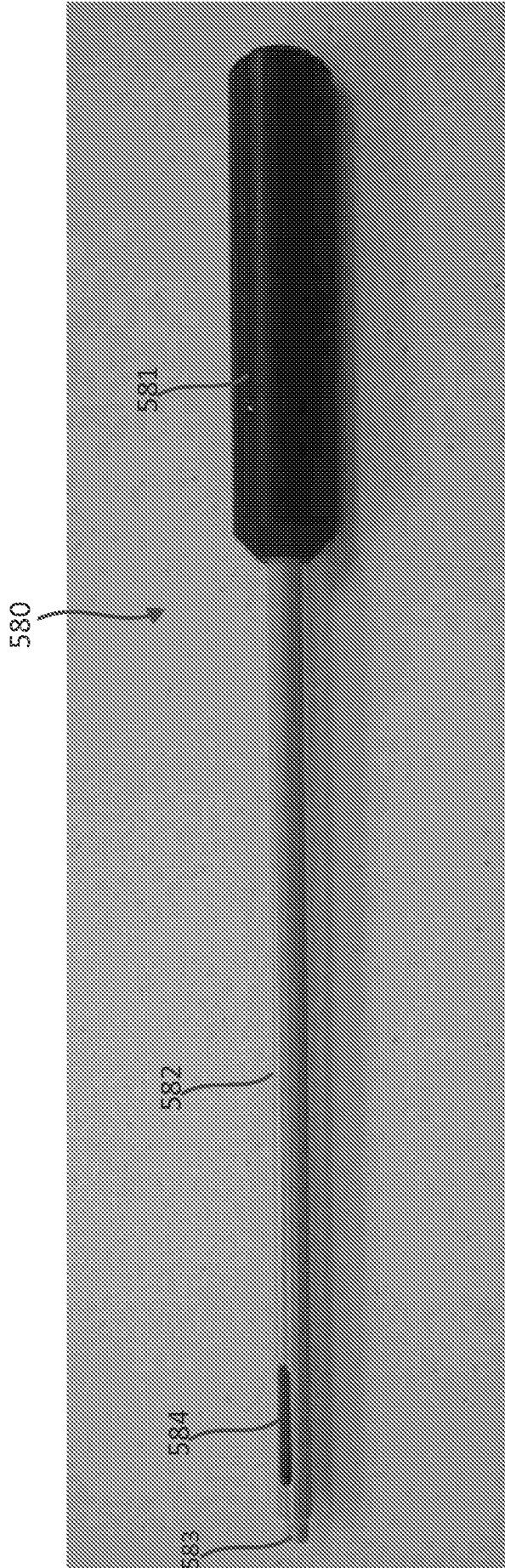


Fig. 32

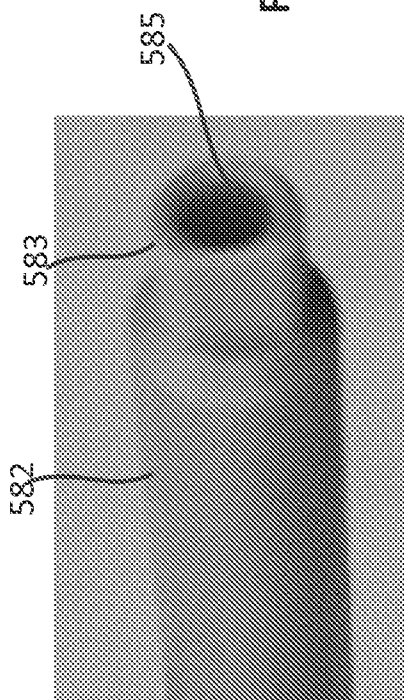


Fig. 33

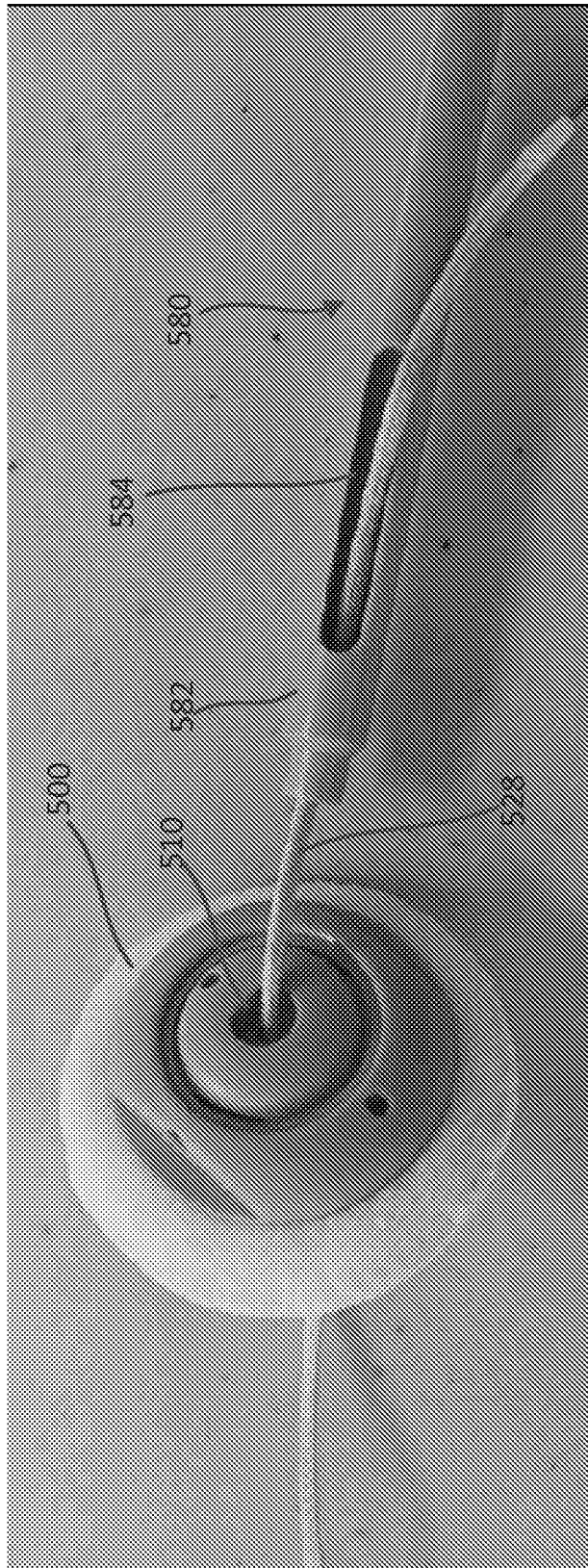


Fig. 34

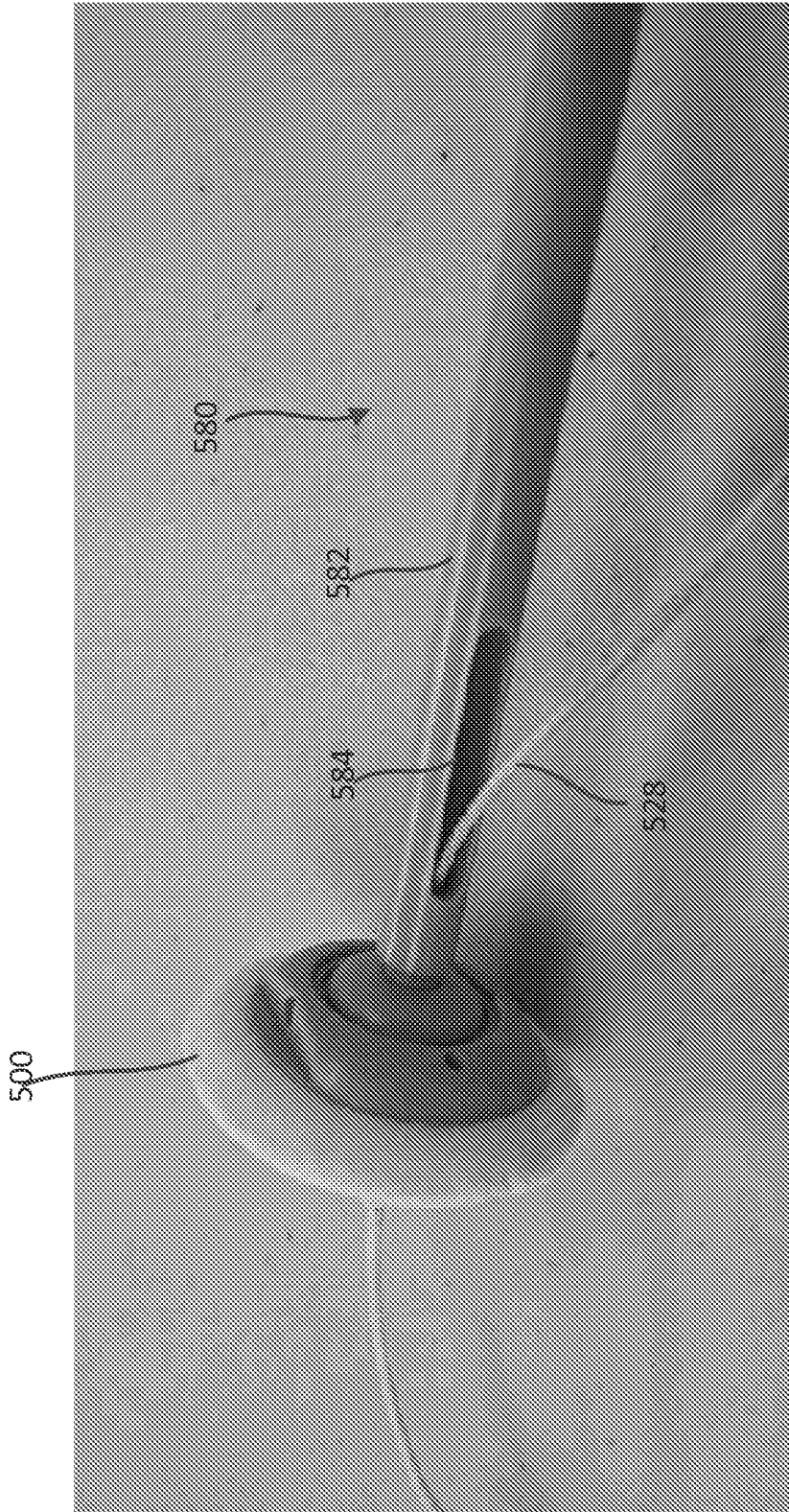


FIG. 35

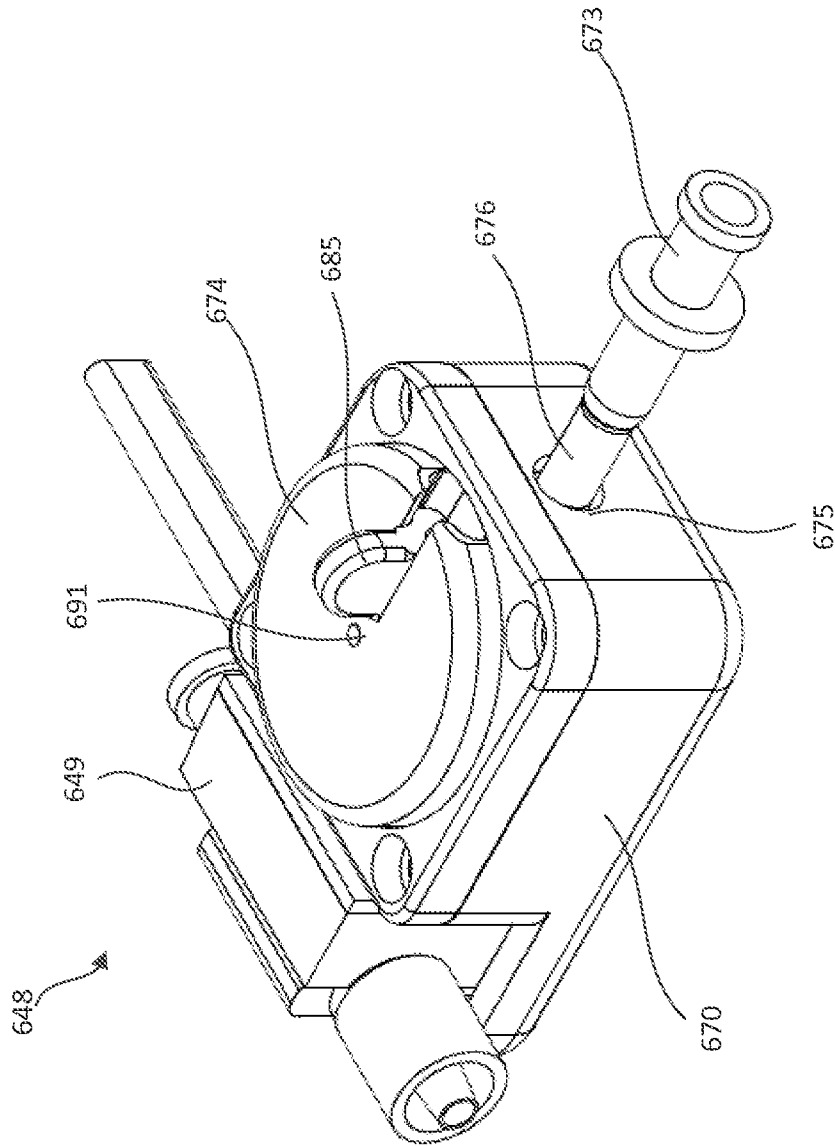


Fig. 36

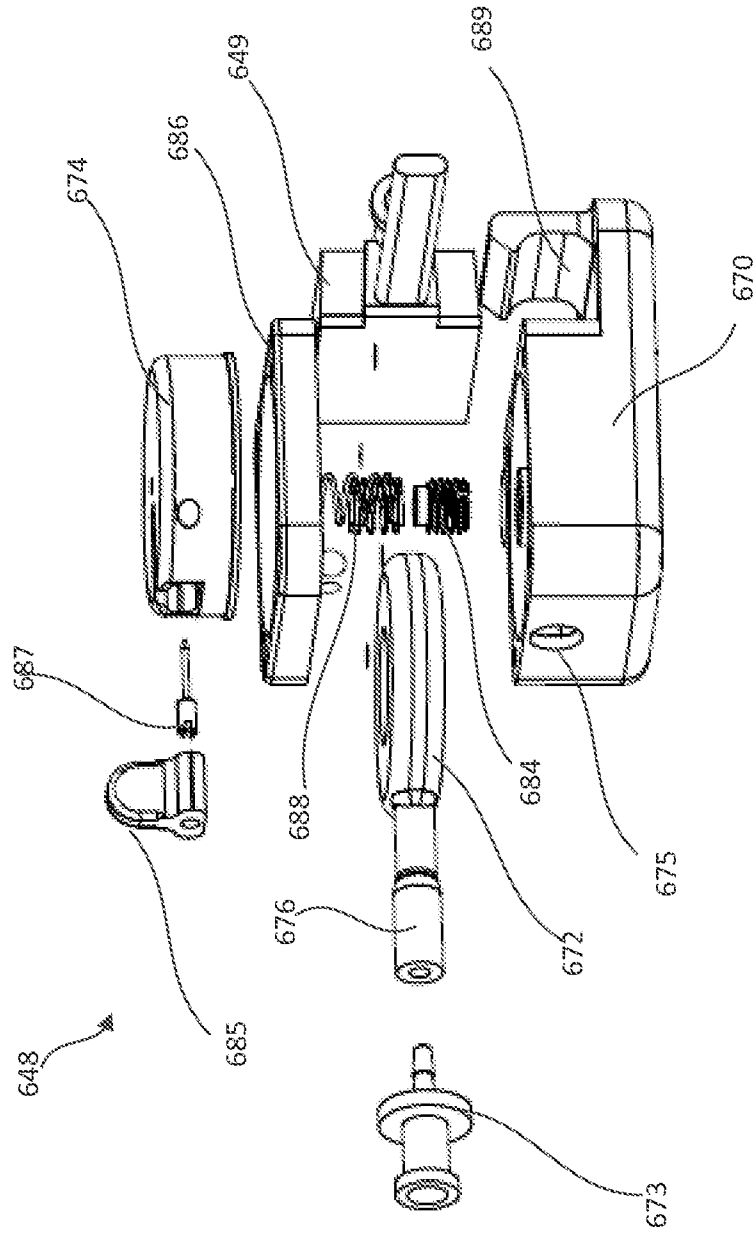


Fig. 37

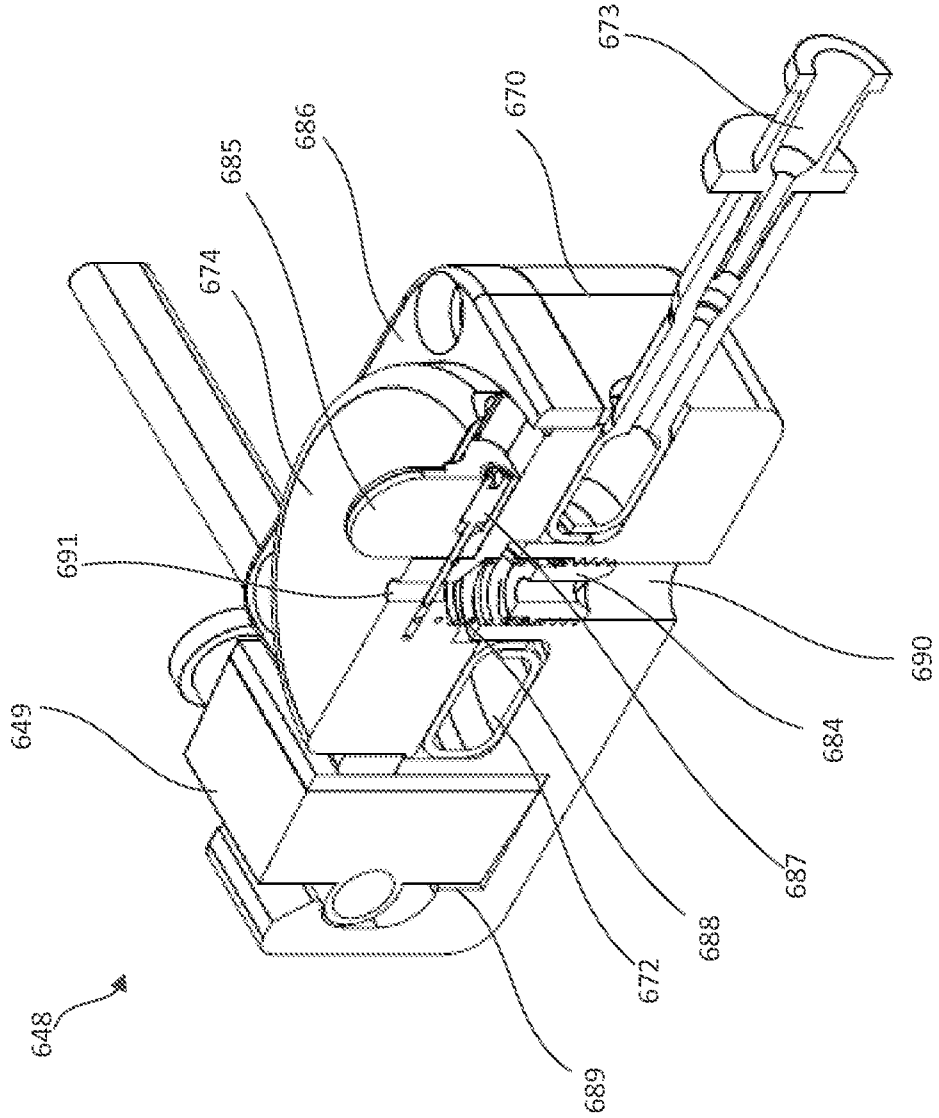


FIG. 38

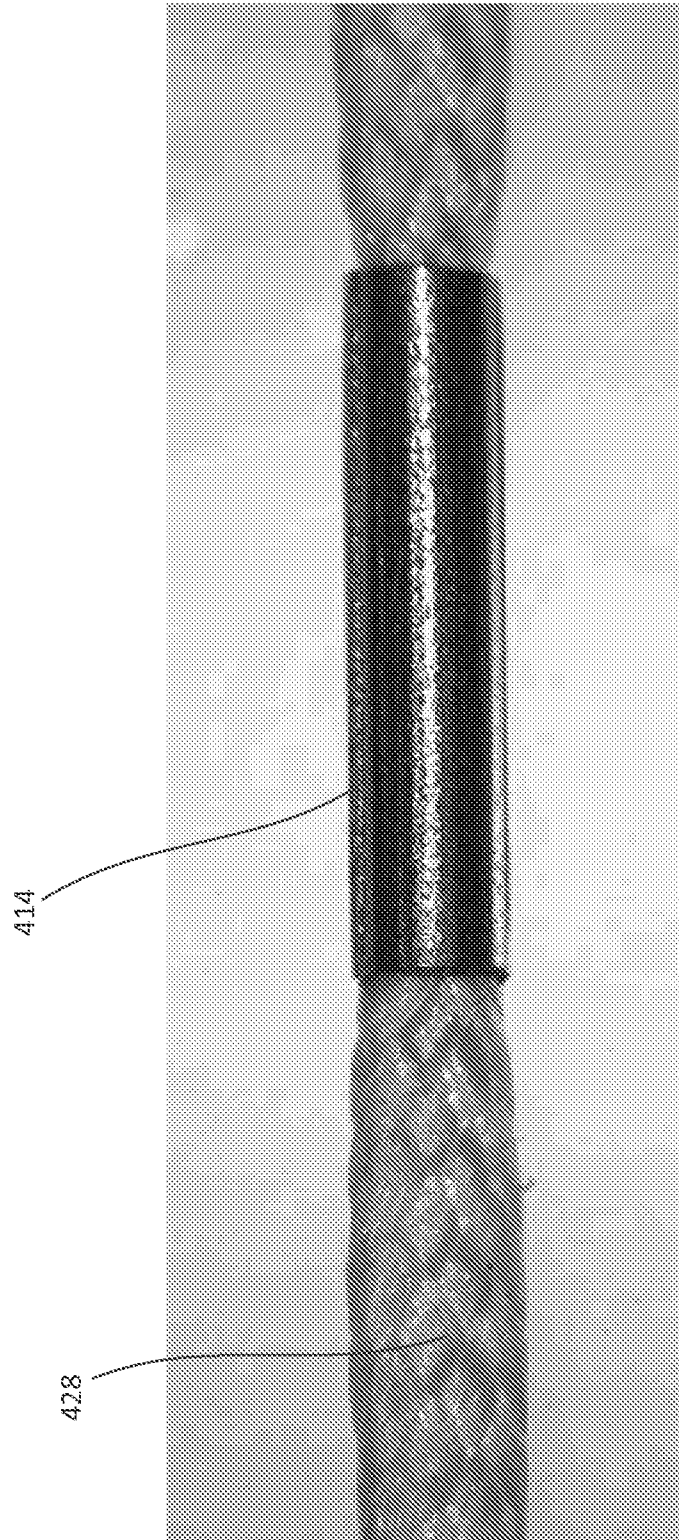


FIG. 39

