CRUSH-RESISTANT TABLETS INTENDED TO PREVENT ACCIDENTAL MISUSE AND UNLAWFUL DIVERSION

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ABSTRACT

Water-insoluble matrix tablets which are capable of prolonged release of active principles liable to be diverted for drug addiction purposes, the said active principles being dispersed within a tabletting matrix composed of at least one excipient selected from the group consisting of pH-independent, water-insoluble delay polymers, inorganic excipients and mixtures thereof, and exhibiting a crush resistance of at least 4 MPa.
**Figure 1**
Dissolution profiles at pH 6.8 of non-film coated 40 mg oxycodone HCl tablets, obtained according to Example 1.

**Figure 2**
Dissolution profiles at pH 6.8 of non-film coated 40 mg oxycodone HCl tablets, obtained according to Example 2.
Figure 3
Dissolution profile at pH 6.8 of tablets conforming to Example 2, film-coated with a layer of Ethylcellulose EC30 D and subjected to a curing step.
Figure 4

Comparative dissolution profiles of oxycodone matrix tablets conforming to the invention in an ethanol-free 0.1 N HCl medium and in a 0.1N HCl medium containing 40% ethanol.
Figure 5
Dissolution profiles of oxycodone matrix tablets conforming to the invention in two dissolution media of different pH (1.2 and 6.8)
Figure 6

24-hour dissolution profiles of 40 mg oxycodone tablets conforming to the invention after a storage period in Al/Al blister pack under accelerated stability conditions of 1 month, 2 months, 3 months and 6 months.
Figure 7
24-hour dissolution profiles of 20 mg oxycodone tablets conforming to the invention after a storage period in HDPE bottles with desiccant under accelerated stability conditions of 1 month, 2 months and 3 months.
Figure 8

Plasma profiles of oxycodone after once-a-day administering of 40 mg oxycodone tablets conforming to the invention, and 40 mg oxycodone tablets of the reference product Oxycontin®

![Graph showing plasma profiles of oxycodone](image)
Figure 9
24-hour dissolution profile of ultra-hard non-coated tablets containing oxycodone and naloxone, at pH 6.8.

Figure 10
10-hour dissolution profiles at pH 6.8 of ultra-hard, non-coated 20 mg oxycodone tablets comprising a matrix containing mineral excipients
Figure 11
Dissolution profiles of tablets conforming to the invention (« QD ») and tablets of the reference product Oxycontin® (ref) at pH 6.8, for whole tablets, tablets cut in half, or crushed (« in pieces »)
Figure 12

Dissolution profile of hydromorphone microgranules in an aqueous medium (0.1 N HCl) under three conditions: without ethanol, in the presence of 20% ethanol and in the presence of 40% ethanol for 4 hours.
Figure 13

Dissolution profile of morphine sulfate microgranules in pH 6.8 dissolution medium without ethanol, at pH 6.8 in the presence of 20% ethanol and at pH 6.8 in the presence of 40% ethanol for 12 hours.
Figure 14

Comparative dissolution tests between ultra-hard morphine sulfate tablets of the invention and commercially available morphine sulfate tablets (Avinza®); A) in 0.1 N HCl medium with 20% ethanol; B) in 0.1 N HCl medium with 40% ethanol

A)

Comparison of dissolution profiles in 0.1N HCl with 20% ethanol (100 rpm, 30 mg/vessel, 500 ml, rotating paddle, UV)

B)

Comparison of dissolution profiles in 0.1N HCl with 40% ethanol (100 rpm, 30 mg/vessel, 500 ml, rotating paddle, UV)
CRUSH-RESISTANT TABLETS INTENDED TO PREVENT ACCIDENTAL MISUSE AND UNLAWFUL DIVERSION

[0001] The present invention concerns insoluble matrix tablets having very high crush resistance.

[0002] These matrix tablets which are unbreakable under usual conditions, non-friable and insoluble in an aqueous medium, are of particular interest as reservoirs for psychotropic agents since they can reduce and even prevent addictive abuse of these substances by crushing, dissolving and injection, or by crushing and inhalation.

[0003] The present invention also concerns the method to obtain said tablets and their use for sustained-release, oral administering of the active ingredients, and in particular of psychotropic active ingredients.

[0004] With respect to tablets containing sustained-release opiate agents, in particular oxycodone, the phenomenon of accidental misuse may assume several aspects. First, it may arise from failure to heed administering conditions. It may happen that the tablet, intended to be swallowed, is accidentally chewed by the patient. The consequences of full or partial destruction of the tablet whose structure is intended to delay the release of the active ingredient, can prove to be dangerous and even fatal for the patient (excess dosage leading overdose). This is the reason why the leaflet supplied with the drug OxyContin® LP specifically states that <<The tablets must be swallowed whole without being chewed>>.

[0005] Also, accidental misuse of drugs containing sustained-release oxycodone has also been observed when patients simultaneously, or within a short time interval, ingest the drug with a strong dose of alcohol.

[0006] It has effectively been observed with a sustained-release form of hydromorphone that the presence of alcohol in the stomach deteriorated the layer of excipients designed for sustained release of the active ingredient, leading to release into the body of a major quantity of active ingredient (<<dose-dumping>>), once again the cause of a dangerous overdose.

[0007] The leaflet supplied with OxyContin® LP for example indicates in the list of contraindications that the consumption of alcohol is to be avoided with this drug.

[0008] Similarly, in the United States, the FDA (Food and Drug Administration) gives a serious warning to patients treated with OxyContin® not to consume alcoholic drinks during the period of treatment (see in particular: http://www.fda.gov/cder/drug/infopage/oxycontin/oxycontin-qg.htm).

[0009] There is therefore a real need to prevent this type of accidental misuse to increase patient safety, whilst maintaining a simple, comfortable route of administration (oral route).

[0010] Since the placing on the French pharmaceutical market in 1990 of substitute treatments for opiate drugs, in the form of sublingual tablets (Temgesic®) initially packed in a form for injection, an increase has been observed in the phenomenon of abuse of certain psychotropic agents by drug addicts.

[0011] The term deliberate misuse or illicit use (or more usually "drug-abuse") is used to qualify the use of certain medicinal products for addiction purposes, in particular the use of certain psychotropic or narcotic agents e.g. opioids or their derivatives intended to treat severe pain or to treat addiction to opiate drugs.

[0012] Abuse by parenteral/nasal route of sustained-release active ingredients normally intended for oral route, gives drug addicts the opportunity to achieve immediate, accumulated psychotropic effects of the total active ingredient dose present in the initial formulation.

[0013] For example, in the particular case of buprenorphine, a powerful opioid analgesic initially sold as a preparation under the name Temgesic® for the substitution treatment of drug addicts; it is estimated that 25% to 30% of the treatments sold are given abuse by parenteral or nasal route. The same applies to the preparation called Subutex® (sublingual tablets with high buprenorphine dosage manufactured by Schering-Plough) officially used as substitution treatment in tens of thousands of opioid drug addicts, for which it is estimated that 34% of consumers abuse the drug by injection and approximately 30% by nasal route.

[0014] Yet the phenomenon of drug abuse is also seen with preparations intended to treat severe pain, such as morphine sulphate (Skenan®) and oxycodone for example (Moscotin®, OxyContin® LP) or moderate pain (Neocodion®). These sustained-release forms contain large quantities of opioids intended to limit pain over long periods, and abuse thereof gives rise to the massive release of morphine derivatives.

[0015] Drug abuse also affects other classes of therapeutic drugs, in particular benzodiazepines (Rohypnol®), and to a lesser extent certain neurological treatments (Artane® Anti-parkinson drug).

[0016] As a result, these therapeutic or substitution treatments, in some cases accessible by mere prescription, and whose dosage can reach up to ten or so tablets a day, are subject to two chief modes of abuse: parenteral administration (injection) and nasal administration (inhalation).

[0017] With regard to abuse by injection, the tablet or capsule containing the active ingredients of interest is reduced to a fine powder using any possible means available to the drug addict, in particular a mortar or lighter, even simply by chewing or biting the tablet. The rough powder obtained, which necessarily contains the excipients initially present in the pharmaceutical form, can then be dissolved in a small volume of liquid (a few millilitres) sometimes previously heated and/ or to which an acid is added for certain active ingredients present in base form (brown heroin, base morphine). The liquid obtained can then be roughly filtered to limit the entry of large particles into the bloodstream, using a cigarette filter for example, before it is injected via intravenous route.

[0018] In this case, the active ingredient then becomes immediately available in the bloodstream, since there is no longer any excipient to delay its release, giving rise to an immediate psychotropic effect sought by drug addicts.

[0019] Abuse by inhalation also consists of crushing the pharmaceutical form until a sufficiently fine powder is obtained to render the active ingredient accessible to the micro-vessels of the intranasal mucous membrane. Here again, the action of the sustained-release excipients, designed for oral administration, is fully ineffective and the expected immediate psychotropic effect is able to be achieved.

[0020] Drug abuse is also accompanied by numerous health risks related directly to injection or inhalation of the excipients and of non-purified crush residues, little or ill-filtered and non-sterile. Recent studies report that some tampered tablets are sometimes dissolved directly in the syringe, then injected without any prior filtering, this practice being directly responsible for numerous deaths through pulmonary embolism.
Additionally, the addition of acids in non-sterile liquid form (lemon juice) to the crush residues is apparently also responsible for the transmission of bacterial or mycosal pathologies (candidiasis).

These practices therefore come to increase the already high risks of viral and bacterial transmissions and complications of dermatological type (abscesses, necrosis) related to the parenteral injection itself. Also, regarding the injection of Subutex® tablets, the presence of corn starch in the tablet formulation is responsible for the onset of oedema due to this excipient which, once injected, accumulates in the lymph and venous systems leading to swelling of the lower limbs.

To limit these problems, one approach consists of associating the active ingredient in one same pharmaceutical form with an agent capable of limiting the psychotropic effect when the formulation is taken by parenteral route.

This is the case for example with formulations combining methadone and naloxone, initially described in U.S. Pat. No. 3,966,940 and U.S. Pat. No. 3,773,955.

This abuse-deterrent formulation was reproduced in the particular case of buprenorphine. Patent EP 0 185 472 for example describes an oral formulation of buprenorphine also containing an effective dose of naloxone, which acts as competing antagonist at the morphine receptors. Since naloxone has only very slight bio-availability via oral route, it little hinders the analgesic action of buprenorphine when the medicinal product is administered conventionally per os. On the other hand, when subject to abuse by parenteral route, naloxone becomes fully available and inhibits the analgesic action of buprenorphine. With this type of chemical association, however, the oral pharmaceutical form remains crushable and soluble in an aqueous medium.

One sublingual formulation combining naltrexone with buprenorphine has also been described in patent EP 0 319 243. With said association, it is possible in particular to increase the antagonist effect of naltrexone with respect to opioids, whilst providing consumers with a non-endorphinergic, analgesic sensation even if the composition is abused by parenteral route. This type of formulation therefore has little appeal for a drug addict and contributes towards curbing the phenomenon of drug abuse. However, this approach necessarily has recourse to the co-administration of two active ingredients, leading to increased production costs and sale price of the medicinal product.

Still using an approach combining the association of the opioid with an antagonist agent, patent application US 2003/0143269 describes a pharmaceutical form in which the opioid and the antagonist are interdispersed so that the antagonist is "sequestered" in a compartment preventing it from being released when the medicinal product is taken normally by oral route. On the other hand, if the product is tampered with by crushing, deterioration of the structure leads to mixing of the two active agents and to inhibition of the sought after psychotropic effect.

In this approach, the pharmaceutical form has a predominant role to play against abuse. However, here again the chemical association of two compounds is necessary, leading to a complex manufacturing process and high production costs.

Also, patent application US 2003/0068392 describes a pharmaceutical form in which the opioid agent is associated not only with an antagonist, but also with an irritant agent sequestered in a closed compartment. Tampering with the pharmaceutical form inevitably leads to release of the irritant. This form therefore requires the association of three active agents, and the creation of compartmented areas, which makes its manufacture complex and more costly than a simple pharmaceutical form such as a tablet.

Other companies have developed pharmaceutical systems in which the opioid or substance which may be subject to abuse is not associated with an antagonist. For example, patent application US 2005/0281748 teaches the manufacture of an oral dosage pharmaceutical form in which the opioid agent of interest is modified so as to increase its lipophilicity, by forming a salt between the active agent and one or more fatty acids.

This pharmaceutical form allows the sustained release of the active ingredient when it is taken by oral route, since the enzymes of the gastrointestinal tract gradually breakdown the groups of fatty acids, releasing the active ingredient as and when they are broken down.

On the other hand, any physical tampering of the pharmaceutical form releases microparticles of active ingredient coated with an insoluble layer, preventing the immediate release of the active ingredient in an aqueous medium. Said formulation requires chemical conversion of the active ingredient.

Patent application US 2003/0118641 describes an oral dosage form of opioid with sustained release, in which the active opioid ingredient is associated with a hydrophilic polymer matrix and a cationic resin. Since the resin carries opposite charges to the active ingredient, it binds to this ingredient within the polymer matrix, preventing its extraction.

Said pharmaceutical form renders the active compound inseparable from the excipients responsible for its sustained release in the body, even if usually available solvents are used (hot water, alcohol, vinegar, hydrogen peroxide, etc. . . .).

Some companies have developed pharmaceutical systems containing gels. For example Pain Therapeutics Inc. and Durco use a biodegradable gel which can be administered via oral or parenteral route, consisting of an agent with high viscosity: Sucrose Acetate Iso Butyrate (SAIB). This gel allows sustained release of an opioid agent, oxycodone. This type of gel, which is the subject of U.S. Pat. No. 5,747,058 and U.S. Pat. No. 6,413,556 maintains its capacity to release the active ingredient controllably over periods of 12 to 24 hours, even if the capsules containing the same are deteriorated or crushed. The main interest of these pharmaceutical forms lies in the fact that the oxycodone cannot be extracted from its gel carrier, and cannot be injected either via parenteral route owing to the very high viscosity of these formulations (Remoxy® product using ORADUR® and SABER® technologies currently undergoing phase III clinical trials).

Said gels also have the capacity to resist extraction of oxycodone in the presence of an alcohol or acid, the active ingredient remaining trapped in the network formed by the gelling agent.

These gel-containing pharmaceutical forms are complex formulations, which firstly require the use of high viscosity liquids at industrial level, giving rise to restricted handling, and secondly entail major restrictions with regard to packaging (use of bottles of vials), which is not the case with tablets.
Means are also known with which to manufacture matrix tablets of very high hardness. Patent EP 0 974 355 describes tablets obtained by granulating a hydrosoluble vitamin mixed with at least one additive of saccharide type, in the presence of a conventional polymer binder such as HPMC for example. Said tablets, intended for swift release of the hydrosoluble vitamin in the body, have high hardness strength, in the order of 20 to 30 kp/cm² (kiloponds/cm²), which is equivalent to hardness values of approximately 1.96 to 2.94 MPa. Although relatively hard and consisting of more than 90% hydrosoluble vitamin and of excipients that are also hydrosoluble (HPMC, saccharides), these tablets disintegrate rapidly in the body (disintegration time in the region of 10 to 15 minutes). Said tablets are firstly fully unsuitable for sustained release of the active ingredient, and secondly are easily dissolved in an aqueous medium, making them unfit for use as pharmaceutical form for substances which may be given abuse.

Patent EP 0 933 079 describes matrix tablets having a crush resistance varying from around 1 MPa (1 N/mm²) up to 10 MPa. Said tablets are obtained from a treated starch powder that can be directly compressed. However, these tablets are intended for the rapid release of active ingredients, since they have a relatively short disintegration time in an aqueous medium, in the order of approximately 6 to 7 minutes. Owing to their rapid disintegration in an aqueous medium these tablets, here again, cannot be used to convey active ingredients which are liable to be given abuse and which are intended to be released over long time periods.

Patent EP 0 997 143 describes the production of bi-convex matrix tablets of very high hardness (up to 1.1 MPa i.e. around 11 kp/cm²) and with a friability of less than 1%, obtained after compressing a matrix consisting chiefly of a compressible, disintegratable carbohydrate (generally mannitol) and a binder. Said chewable tablets, even if they have very high hardness in the solid state, dissolve in an aqueous medium and after a very short period of time in the mouth, and therefore rapidly release the active ingredient into the body.

The manufacture of matrix tablets intended for the sustained release of an active substance in the body, and also having high hardness, is taught by U.S. Pat. No. 6,592,901. In this document, tablets are obtained having good compressibility characteristics and containing a particular grade of ethylcellulose (non-ionic ethyl ether of cellulose—sold under the trade name Aquolan®), that is pH-independent, highly substituted and of low viscosity. The crush resistance of the tablets thus obtained is in the order of 10 to 20 kp (kiloponds) which, scaled down to the size of the tablets, is equivalent to around 1.4-2.8 MPa. Also, this special grade of ethylcellulose is water-insoluble, limiting the diffusion of liquids and hence release of the active ingredient in the body. Release of the active ingredient is achieved slowly since the tablets obtained from this model show a release profile in which less than 80% of the active ingredient is released after 24 hours.

Matrix tablets having very strong crush resistance are also described in the work by Pontier et al. (Pontier et al. Journal of European Ceramic Society 22 (2002)). In particular, the authors show that it is possible to obtain very hard matrix tablets using mineral excipients of the calcium phosphate family, such as tricalcium phosphate or hydroxyapatite, by direct compression. For example, from a tricalcium phosphate powder, previously granulated then compressed under compression forces in the order of 300 MPa, it is possible to obtain tablets whose crush resistance (tensile strength) can reach 6.5 MPa. However, this article does not give any information on the capacity of such tablets to release one or more active ingredients over an extended period of time, nor the capacity of such pharmaceutical structures to remain intact in an aqueous medium.

Thesis research on apatitic calcium phosphate compression by C. Pontier ("Les phosphates de calcium apatiques en compression. De la chimie aux qualités d’usage "Thèse de l’Université de Paris XI, presented on 25 Sep. 2001) shows that it is possible, after compression, to obtain matrix tablets containing calcium phosphates (hydroxyapatite and tricalcium phosphate in particular), having very high crush resistance possibly reaching 7 MPa.

Said tablets also have the capability of releasing theophylline in an aqueous medium over a long period of time (60% of active ingredient released in 8 hours) by gradual diffusion through the matrix pores. However, this article does not allow any conclusion to be drawn on the capacities of said tablets to remain intact in an aqueous medium, and hence to resist abuse by crushing in a liquid medium.

Patent application US 2005/0051546 concerns an abuse-deterrent pharmaceutical form containing one or more active ingredients liable to give rise to addiction, and at least one synthetic or natural polymer necessarily having a tensile strength of at least 500 N. The only polymer specifically described is ethylene polyoxide having a molecular weight of 7 000 000 optionally associated with an xanthane gum. These tablets can be prepared using a method which comprises a compression step preceded by a heat exposure step, concomitant with a heat exposure step or followed by a heat exposure step. Therefore the heat exposure step is necessary to obtain the desired hardness. This step, even if of short duration, is firstly not applicable to heat-sensitive active ingredients and secondly requires the use of special equipment and extra energy consumption which contributes towards increasing the cost of the process.

There is therefore a true need for the development of a pharmaceutical form which allows the safe administering of active ingredients having a psychotropic effect and which are released over an extended period of time i.e. which has a pharmaceutical structure which makes both its crushing and its dissolution highly difficult or even impossible, and further which prevents the extraction and separation of the active ingredient from the agents responsible for its sustained release. In addition, it must be possible for this pharmaceutical form to be produced using an extremely simple manufacturing method, that is rapid and low cost.

The applicant has unexpectedly found a novel, solid, oral pharmaceutical formulation prepared simply in the form of sustained-release matrix tablets, that are both insoluble and ultra-hard. With said tablets, it is possible to prevent the phenomenon of accidental misuse and to curb and even eliminate the phenomenon of drug abuse.

The subject-matter of the invention is therefore water-insoluble matrix tablets, capable of releasing one or more active ingredients into the body over extended periods, preferably over periods of more than 12 hours and further preferably more than 20 hours, containing at least one active ingredient which may be the subject of drug abuse dispersed.
in a compression matrix, said matrix consisting of at least one excipient chosen from the group comprising sustained-release, water-insoluble, pH-independent polymers, mineral excipients and their mixtures, the quantity of said excipient and the compression conditions being chosen so that said tablets have a crush resistance of at least 4 MPa, advantageously at least 6 MPa.

[0048] Advantageously, the compression conditions do not necessarily entail a heating step of the mixture to be compressed, or of the compression tooling either before or during the actual compression step.

[0049] Preferably the tablets conforming to the invention are used to produce pharmaceutical forms capable of releasing the active ingredient or ingredients they contain, in particular opioid agents, over a period of 24 hours, making it possible for these active ingredients to be taken once-a-day.

[0050] Under the present invention, the terms deliberate misuse or drug abuse are used to designate any intentional deterioration of pharmaceutical forms. In particular, the notion of drug abuse concerns reducing the tablets to powder, then inhaling this powder or dissolving it in a small quantity of liquid for its parenteral injection.

[0051] The term matrix tablet is used to designate a tablet whose inner structure is homogeneous and identical from the core towards the periphery of the tablet. Therefore the tablets of the present invention consist of a homogeneous mixture of active ingredient in powder or granule form and of a compression matrix containing at least one excipient chosen from the group comprising sustained-release, water-insoluble, pH-independent polymers, mineral excipients and their mixtures.

[0052] Under the present invention, the term compression matrix is used to designate all the excipients which take part in the cohesion of the tablet. Said compression matrix is both water-insoluble and has a certain permeability (hydrophilic matrix) or a porous network (inert matrix) responsible for gradual release of the active ingredient, which does not vary in relation to the pH conditions of the medium.

[0053] The term << compression mixture >> in the present application is used to designate all the components of the tablet (the active ingredient or ingredients, whether granulated or not, and the constituents of the compression matrix) before their compression into tablet form.

[0054] In the present application, the notions of crush resistance and hardness are both used to characterize the tablets. Hardness characterizes the tensile strength of the tablet under a diametral-compression test. A round tablet is placed between two jaws, one of which is fixed and the other mobile. Hardness corresponds to the force applied by the mobile jaw which causes rupture of the tablet into two more or less equal parts. It is expressed in Newtons (N) or Kilonewtons (kN) (see European Pharmacopoeia: ref: 01/2005:20908).

[0055] Crush resistance is inferred from measurement of hardness: it is a parameter which takes into account the surface area of the tablet exposed to the force, and corresponds to strength per unit surface area expressed in Pascals (Pa) or Megapascals (MPa), 1 MPa corresponding to 1 Newton per mm². Crush resistance is a parameter of particular interest to compare the behaviour of tablets with different surface areas, since it does not require recourse to the parameter of tablet size. Its calculation formula is the following (as per << Determination of tablet strength by the diametral-compression test >>, Fell, J. T.; Newton, J. M. J. Pharm. Sci., 59 (5): 688-691 (1970));

\[
R_d = \frac{2xF}{\pixDh}
\]

in which:

- \(R_d\) is the diametral tablet breaking load (in MPa)
- \(F\) is the hardness of the tablet (in N)
- \(D\) is the diameter of the tablet (in mm)
- \(H\) is the thickness of the tablet (in mm).

[0060] In the present application, the expression << sustained-release >> polymers is used to designate polymers routinely used in the pharmaceutical industry to control the release of an active ingredient into its dissolution medium. In the present application, the sustained-release polymers used are water-insoluble, which means that release of the active ingredient into the surrounding medium occurs exclusively via a phenomenon of simple diffusion, with no erosion or gradual disintegration of the polymer. These polymers effectively have certain permeability vis-à-vis the surrounding medium, responsible for gradual diffusion of the active ingredient out of the polymer matrix. Therefore the lower the permeability of the polymer, the more the diffusion of the active ingredient is sustained.

[0061] Under the present invention, the expression pH-independent polymers is used to designate those polymers capable of forming a permeable network or matrix, and whose permeability is not influenced by the pH of the surrounding medium.

[0062] The tablets of the invention are tablets with very high hardness (hereunder called << ultra-hard tablets >>). Their structure is such that their crushing cannot be envisaged using conventional domestic techniques, and their dissolution in an aqueous medium, even an acidified medium, is practically impossible.

[0063] This extreme hardness is also accompanied by little or no friability, which means that these tablets are a pharmaceutical form of choice for active ingredients likely to be the subject of drug abuse, such as psychotropic agents for example. This very low or non-friability makes the tablets practically unbreakable using conventional or domestic techniques (spoon, mortar, lighter . . . ).

[0064] The tablets of the invention are also practically insoluble in an aqueous medium, even at low pH (pH < 3). These characteristics make them difficult to administer via parenteral route.

[0065] The tablets of the invention are also insoluble in an alcoholic medium, which means that they can be taken even if alcohol is ingested, thereby avoiding accidental misuse.

[0066] Additionally, the tablets of the invention, despite their extremely hard, resistant outer structure, allow sustained release of the active ingredient or ingredients contained in said matrix. The tablets of the invention therefore allow release of the active ingredient into the body over a period that is greater than 8 hours, preferably greater than 12 hours, further preferably greater than 20 hours.

[0067] Advantageously, the tablets of the invention are used to produce pharmaceutical forms of opioid agents having once-a-day administration.

[0068] Finally the matrix structure of the tablet according to the invention, consisting of a mixture of known sustained-release excipients approved for oral use and of granules containing the active ingredient, is extremely simple, allowing for its easy industrial production since it requires a simple
compression step of the mixture without the need to heat the compression tooling and/or mixture to be compressed either before or during the actual compression step.

[0069] Advantageously, the compression matrix of the tablets conforming to the invention represents 50 to 98 weight % of the total weight of the tablets, further advantageously 85 and 95 weight % of the total weight of the said tablets.

[0070] The excipients, which can be used alone or in a mixture in the matrix composition of the tablets of the invention, can be of organic type; they then belong to the group comprising cellulose derivatives and in particular microcrystalline cellulose (e.g. that sold under the trade name Avicel®) and ethylcellulose (e.g. that sold under the trade name Aquacel®), the polymers of the family of water-insoluble, pH-independent methacrylic acids, in particular the grades Eudragit® RL 12.5, RL PO & RL 100 & RS 12.5, RS PO and RS 100, the derivatives of polyvinylalcohols, the polymers of lactic and glycolic acids (PLGA), starches, waxes, derivatives of polyvinyl acetate, derivatives of polyvinylpyrrolidone and mixtures of polymers such as the mixture of microcrystalline cellulose and [polyvinyl acetate/polyvinylpyrrolidone (80:20)] (sold under the trade name Kollidon SR®) and the mixture of microcrystalline cellulose and [poly(ethylacrylate/methylmethacrylate/trimethylaminoethyl methacrylate chloride) (1:2:0.2)].

[0071] Advantageously, the sustained-release, water-insoluble, pH-independent polymers of the present invention belong to the group comprising cellulose derivatives, the mixture of microcrystalline cellulose and [polyvinyl acetate/polyvinylpyrrolidone (80:20)] (sold under the trade name Kollidon SR®) and the mixture of microcrystalline cellulose and [poly(ethylacrylate/methylmethacrylate/trimethylaminoethyl methacrylate chloride) (1:2:0.2)].

[0072] The excipients of the compression matrix can also be of mineral type: they then belong to the group comprising calcium phosphates (in particular dicalcium or tricalcium phosphates), aluminium and silicon silicates, and magnesium carbonates.

[0073] The compression matrix of the tablets according to the invention can advantageously consist of a mixture of several of the above-mentioned excipients. It may be a mixture of organic polymers such as microcrystalline cellulose and of vinyl derivatives in variable proportions, or a mixture of organic polymer+mineral derivative such as a mixture of calcium and silicon silicate-microcrystalline cellulose in variable proportions.

[0074] The excipients present in the compression matrix of the tablets conforming to the present invention advantageously represent between 40 and 100 weight % of the total weight of said matrix, advantageously 50 to 90 weight % of the total weight of the matrix.

[0075] According to one advantageous embodiment of the invention, the compression matrix consists of a (1:1) mixture of two polymers, advantageously it consists of a (1:1) mixture of microcrystalline cellulose and of the mixture [polyvinyl acetate/polyvinylpyrrolidone to a proportion of 80:20 (sold under the trade name Kollidon SR®)], or a mixture of microcrystalline cellulose and [polyethylene/methylmethacrylate/trimethylaminoethyl methacrylate chloride in proportions of (1:2:0.2)]. Advantageously, these two polymers each represent a weight proportion in the order of 40% of the total weight of said compression matrix.

[0076] The compression matrix can advantageously, in addition to the excipients of the compression matrix, contain one or more excipients intended to promote the conducting of the compression process such as anti-adherent agents e.g. colloidal silica, talc, magnesium stearate, Polyethylene Glycol (PEG) or calcium stearate, or to promote cohesion of the tablets on compressing such as binders conventionally used for this purpose, in particular starches, cellulose derivatives, or fillers, lubricants, plasticizers, bulking agents, or sweeteners or colouring agents.

[0077] If present, these excipients are used conventionally to the proportion of 0.1 to 10 weight % of the total weight of the compression matrix, preferably between 0.5 and 5 weight %.

[0078] Said compression matrix may also comprise at least one of the following substances (a) to (f) or a mixture thereof:

[0079] (a) a substance which irritates the nasal and/or pharyngeal tracts,

[0080] (b) an agent increasing viscosity, allowing the formation of a gel when the tablet is dissolved in a minimum amount of water,

[0081] (c) an antagonist of the active ingredient(s) which may be subject of drug abuse,

[0082] (d) an emetic substance,

[0083] (e) a colouring agent as aversive agent,

[0084] (f) a bittering substance.

[0085] If the active ingredient is a natural or synthetic opiate derivative, the antagonist is advantageously chosen from the group comprising naloxone, naltrexone, nalmenfene, nolid, naloxone, nalorphine and naltorphine, these different compounds each being either in a pharmaceutically acceptable form, in particular a base or salt, or solvated form. These antagonists are present in doses conventionally used, in particular to the proportion of 0.5 to 100 mg per tablet.

[0086] In one advantageous embodiment of the invention, said antagonist agent is naloxone or one of its pharmaceutically acceptable salts.

[0087] The tablets conforming to the invention are therefore of particular interest as reservoirs for active ingredients which may be given drug abuse, and which are intended to be released into the body over periods of more than 8 hours, preferably more than 12 hours, and further preferably more than 20 hours.

[0088] The active ingredients contained in the tablets of the invention can be present in any form known to those skilled in the art, in particular in powder, crystal or granulate form.

[0089] The tablets conforming to the invention may contain one or more active ingredients which may be of any type. Advantageously these active ingredients are chosen which are intended to be controllably released into the body i.e. over periods of at least 8 hours and preferably more than 12 hours, further preferably more than 20 hours.

[0090] Preferably, the tablets of the invention are used to produce once-a-day pharmaceutical dosage forms.

[0091] In particular, the tablets of the invention are fully adapted for the sustained release of active ingredients which may be given drug abuse and/or more generally any active ingredients whose rapid or immediate release into the body caused by tampering with the pharmaceutical form could be dangerous or fatal for the consumer.
Therefore, the tablets conforming to the invention are preferably used for the sustained release of active ingredients belonging to the family of psychotropic agents i.e. capable of acting on the psyche by stimulating, tranquilizing or hallucinogenic effects.

Therefore, the active ingredients which can be used under the present invention are preferably derivatives and/or alkaloids of opium, whether natural or synthetic, such as codeine, norcodeine, noscapine and their salts.

The active ingredients which can be used in the invention also belong to the group comprising morphine, its derivatives and their salts, in particular morphinones such as phecodeine, nalorphine, codeine, dihydrocodeine, hydromorphone, and morphinones such as buprenorphine, butorphanol, dextromethorphan, nalbuphine, naltrexone, naloxone, nalmefene, hydrocodone, oxymorphone and oxycodone, and in general all analogs of morphine and all morphine analogsics such as fentanyl, tramadol, apomorphine and etorphine.

The present invention also relates to alkaloid derivatives, whether natural or synthetic, having a psychotropic effect such as cocaine or heroin.

Finally, the present invention also relates to any substances currently used for therapeutic purposes to treat addiction to opiate drugs and/or as substitution and disintoxication treatment, such as methadone and buprenorphine for example, highly subject to drug abuse.

In general, the present invention can also be considered for all other therapeutic classes of medicinal products that are currently the subject of drug abuse, in particular neuroleptics, tranquilizers, hypnotics, analgesics, anxiolytics, and in particular the class of benzodiazepines.

The active ingredient(s) in the tablets of the invention can represent between 5 and 70 weight % of the total weight of the tablet. Advantageously the active ingredient(s) represent 10 to 50 weight % of the total weight of the tablet. The active ingredient(s) can be added directly to the mixture to be compressed, coated on carriers (to obtain microgranules) or wet- or dry-granulated (to obtain granules).

If the active ingredient(s) are in the form of microgranules, these microgranules can be obtained conventionally by depositing (coating) the active ingredient(s) on the surface of pharmaceutically neutral carriers, such as pre-manufactured microspheres containing cellulose or a mixture of sugar and starch sold under the name "neutral cores" or "sugar spheres", or they may be granules of other excipients such as lactose for example.

The depositing (coating) method of the active ingredient is a conventional method known to those skilled in the art and may vary in relation to the type, quantity and fragility of the active ingredient(s) to be deposited. Therefore depositing (coating) can be made by spraying a solution or suspension of the active ingredient(s) onto the surface of the neutral carrier, or by spraying the active ingredient(s) in powder form onto the surface of the carrier previously moistened with a binder solution.

The granules of active ingredient(s) may also be obtained by dry or wet granulation of the active ingredients of interest, generally in the presence of at least one binding agent and optionally a wetting agent, depending on techniques, here again well known to those skilled in the art.

The granules thus obtained are mixed with the excipients of the compression matrix, and the mixture is then compressed.

The exceptional hardness of the tablets conforming to the invention can be obtained without it being necessary to apply a heating step, before or during compression, to the mixture to be compressed (compression matrix and active ingredient) and/or to the compression tooling (press).

Advantageously, the granules containing the active ingredient(s) of interest have a diameter allowing a good compression yield, i.e. generally between 100 and 600 µm.

According to another embodiment of the invention, and if particle size so permits, the active ingredient is mixed directly with the excipients forming the compression matrix, then the mixture is directly compressed.

Finally, another possibility of the invention consists of mixing the active ingredient with the excipient(s) of the compression matrix, then dry- or wet-granulating this mixture to obtain directly compressible granules.

The tablets conforming to the invention can be of any shape and size allowing tablets of high hardness to be obtained. Advantageously the total surface area of the tablet is less than 150 mm².

The present invention is therefore suitable for the production of tablets with either low or high doses of active ingredient.

According to one particular embodiment of the invention, the tablets can be film-coated with an outer coating which those skilled in the art will know how to adapt in relation to needs and the intended function of this coating.

For example, the outer coating can be applied for the purpose of protecting the active ingredient, if it is a labile active ingredient sensitive to the low pH values of the gastric medium for example, in which case the term gastroresistant coating is used.

Also, the outer coating can be applied to further delay diffusion of the active ingredient through the matrix. For this purpose different grades of ethylcellulose can be used, or of methacrylic polymers well known to the skilled person.

Finally, the outer coating can be used to modify the cosmetic appearance of the tablet (texture, colour) and/or palatability (taste/feel in the mouth) for the patient. In particular, excipients can advantageously be used such as cellulose derivatives or acrylic derivatives well known to those skilled in the art, to mask the taste of the active ingredient if necessary.

Said coating can therefore consist of a mixture of one or more excipients of different type known to those skilled in the art, used either alone or in a mixture for the different functions listed above.

The excipient(s) used for coating are applied in a manner known to those skilled in the art, in the necessary quantity to obtain the desired function(s).

These excipients can be applied to the surface of the tablet in conventional manner by spraying a solution or suspension of coating agent in a solvent, in a perforated pan or fluidized bed for example.

The present invention also concerns the method to manufacture the tablets of the invention. This method comprises the following steps:

- mixing the active ingredient(s) with the excipient(s) of the compression matrix,
- optional granulation, and
- compressing said mixture under conditions chosen so that said tablet has a crush resistance of at least 4 MPa, advantageously at least 6 MPa,
- optional coating of the tablet.
If the coating polymer of the tablet is a sustained-release polymer, the coated tablets conforming to the invention can advantageously undergo a curing step of said coating polymer to guarantee its physical and chemical stability. This step is conducted under controlled temperature conditions, below the melt temperature of the active ingredient, and for a controlled time which is dependent upon the coating polymer and which may last between 1 minute and several months, for a relative humidity rate of 50 to 99%. This step can be conducted in an oven or pan.

The active ingredient can be mixed directly in the compression matrix, or mixed in the form of previously prepared granules or microgranules. This granulation step improves the uniform resistance of the tablets produced. Preferably, for granules, wet-granulation is used (aqueous or organic), or for microgranules the active ingredient is deposited by spray-coating in solution or suspension onto neutral carriers.

Compression is performed on a rotary compressing machine with pre-compression station. The compression parameters must be chosen so that the hardness of the tablets obtained is adapted to the present invention. However, it is not necessary to apply any heating step either before and/or during compression to the mixture to be compressed or to the compression tooling, for the purpose of achieving the exceptional hardness observed with the tablets of the invention. The applied compression forces lie between 10 kN and 160 kN, advantageously between 30 kN and 80 kN. They are chosen to be compatible with the punch material and so that they can be used at industrial production rates, whilst allowing tablets to be obtained whose tensile strength is greater than 4 MPa, and preferably greater than 6 MPa.

Examples 1 to 10 and FIGS. 1 to 14 given below are intended to illustrate the invention but do not in any way limit its scope.

FIG. 1 gives the dissolution profile in phosphate buffer medium pH 6.8 (monopotassium phosphate/disodium phosphate) of 40 mg oxycodone HCl tablets, non-film coated, obtained according to example 1.

FIG. 2 gives the dissolution profile at pH 6.8 of non-film coated, 40 mg oxycodone HCl tablets, obtained according to example 2.

FIG. 3 gives the dissolution profile in phosphate buffer medium pH 6.8 (monopotassium phosphate/disodium phosphate) of tablets conforming to example 2, film-coated with a layer of ethylcellulose E.C30 D, which have undergone curing under the conditions of example 3.

FIG. 4 gives the comparative dissolution profiles of oxycodone matrix tablets according to the invention in an ethanol-free 0.1 N HCl medium, and in a 0.1 N HCl medium containing 40% ethanol such as measured according to example 4.

FIG. 5 illustrates the dissolution profiles of oxycodone matrix tablets conforming to the invention in two dissolution media of different pH (1.2 and 6.8) following the operating mode described in example 4.

FIG. 6 illustrates the 24-hour dissolution profiles of 40 mg oxycodone tablets according to the invention, after a storage period in ato/ato blister packs under accelerated stability conditions of 1 month, 2 months, 3 months and 6 months under the conditions of example 4.

FIG. 7 illustrates the 24-hour dissolution profiles of 20 mg oxycodone tablets conforming to the invention, after a storage period in HDPE bottles with a desiccant under conditions of accelerated stability of 1 month, 2 months and 3 months.

FIG. 8 gives the plasma profiles of oxycodone after once-a-day administration of 40 mg oxycodone tablets conforming to the invention, and 40 mg oxycodone tablets of the reference product OxyContin®, according to example 4.

FIG. 9 illustrates the 24-hour dissolution profile, at pH 6.8, of ultra-hard, non-coated tablets of oxycodone and naloxone, according to example 5.

FIG. 10 illustrates the 10-hour dissolution profiles, at pH 6.8, of non-coated, ultra-hard tablets containing 20 mg oxycodone.

FIG. 11 illustrates the dissolution profiles observed with tablets conforming to the invention (<<OIT>> ) and tablets of the reference product OxyContin® (rel) at pH 6.8, for whole tablets, tablets cut in half or crushed tablets (<<in pieces>>).

FIG. 12 gives the dissolution profile of microgranules of hydromorphone in an aqueous medium (0.1 N HCl) under three conditions of dissolution: without ethanol, in the presence of 20% ethanol and in the presence of 40% ethanol, for 4 hours according to the conditions of example 9.

FIG. 13 gives the dissolution profile of microgranules of morphine sulphate in a dissolution medium of pH 6.8 without ethanol, at pH 6.8 in the presence of 20% ethanol, and at pH 6.8 in the presence of 40% ethanol for 12 hours, according to example 10.

FIG. 14 illustrates comparative dissolution tests between ultra-hard tablets of morphine sulphate conforming to the invention, and commercially available tablets of morphine sulphate (Avinza®) in the presence of: A) 20% ethanol in 0.1 N HCl medium, or B) 40% ethanol in 0.1 N HCl medium, according to example 10.

EXAMPLE 1

Manufacture of Tablets Containing Granules Obtained by Granulating Oxycodone HCl and 4.87% HPMC and Containing a Compression Matrix Consisting of a 1:1 Mixture of Two Excipients [Microcrystalline Cellulose and (PVA/Povidone 80:20)]

1. Preparation of the Tablets

1.1 Preparation of Oxycodone Granules

The granules are obtained by wet granulation of the active ingredient (oxycodone HCl, batch No. DV000165; McFarlan Smith, England) and hydroxypropylmethylcellulose (HPMC grade Pharmacoat® 606, Brenntag) which acts as binder. Granulation is conducted in a fluidised bed (GCPG-1, Wurster, Glatt, Germany) by bottom-spraying a solution of the binder (HPMC) onto the active ingredient in powder form.

Oxycodone is added to the fluidised bed and placed in sustainedisation. The binder solution is sprayed onto the powder which aggregates to form granules. Water is progressively removed by evaporation and after a final drying step. The final drying step is in an oven (16 hours at 60°C) is conducted to obtain an acceptable final water content (less than 6%).
The proportions of HPMC and oxycodone are given in Table 1.

### TABLE 1

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Percentage [%]</th>
<th>Wt. in grams/batch</th>
</tr>
</thead>
<tbody>
<tr>
<td>Oxycodone HCl</td>
<td>95.13</td>
<td>500.0</td>
</tr>
<tr>
<td>HPMC (Pharmachol® 606)</td>
<td>4.87</td>
<td>25.6</td>
</tr>
<tr>
<td>Purified water</td>
<td></td>
<td>336.9</td>
</tr>
<tr>
<td><strong>Total (dry)</strong></td>
<td><strong>100.0</strong></td>
<td><strong>525.6</strong></td>
</tr>
</tbody>
</table>

The granules obtained after the fluidised bed step have the characteristics indicated in Table 3.

### TABLE 3

<table>
<thead>
<tr>
<th>Batch number</th>
<th>Mean particle size (μm)</th>
<th>Apparent density g/mL</th>
<th>Flow time (Sec./100 g)</th>
<th>Relative humidity (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>XOOXY4979</td>
<td>108.7</td>
<td>0.450</td>
<td>6</td>
<td>3.47</td>
</tr>
</tbody>
</table>

1.2. Preparation of the Compression Matrix

A pre-mixture of microcrystalline cellulose (Avicel® PH102, FMC) and precipitated silica (Sylloid® 244, Keyser & Mc Kay) is formed in a cubic mixer (AR 401, Erweka) for 2 min at 40 rpm. The mixture of polyvinylacetate/povidone (80:20) (Kollidon® SR, BASF) and the oxycodone granules prepared as described under step 1.1 are added to the pre-mixture and homogenisation is conducted in the cubic mixer for 15 minutes at 40 rpm. Finally, the lubricant (magnesium stearate, Quindis) intended to limit sticking and friction during compression is added to the preceding mixture using the mixing parameters: 5 minutes at 40 rpm.

The quantity of oxycodone granules used is determined with a view to producing tablets containing 40 mg oxycodone.

1.3. Compression

The compression step of the final mixture obtained in the preceding step is conducted on a compression press (PR-12, Sviec) with a compression force of 35 kN using oblong punches 11 mm x 5 mm. Compression is conducted conventionally, without the mixture to be compressed or the compression tools being subjected to a heating step either before or during the actual compression step.

The characteristics of the tablets obtained are summarized in Table 5. The mean values correspond to the mean calculated for 20 tablets.

### TABLE 4

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Percentage [%]</th>
<th>Weight (mg/tablet)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Oxycodone granules</td>
<td>19.83</td>
<td>44.62</td>
</tr>
<tr>
<td>(XOOXY4979)</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Kollidon® SR</td>
<td>39.74</td>
<td>89.40</td>
</tr>
<tr>
<td>Avicel® PH102</td>
<td>39.73</td>
<td>89.40</td>
</tr>
<tr>
<td>Sylloid® 244</td>
<td>0.20</td>
<td>0.45</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>0.50</td>
<td>1.13</td>
</tr>
<tr>
<td><strong>Total</strong></td>
<td><strong>100.00</strong></td>
<td><strong>225.00</strong></td>
</tr>
</tbody>
</table>

1.4. Dissolution Profile of the Tablets Obtained According to Example 1

The tablets obtained according to Example 1 have very high hardness, 6 Mpa, and zero friability, without the need to heat the matrix constituents or the compression press before or during compression.

Additionally, the applicant has evidenced that these tablets are practically insoluble in an aqueous medium, even if acid: on completion of the dissolution tests (over 24 h) the tablets remain intact at the bottom of the dissolution vessel, both in a pH 6.8 buffered medium, and in a pH 1.2 acid medium.
2. Dissolution Method

[0153] Measurement of the dissolution of the tablets obtained in Example 1 is performed in 900 mL of dissolution medium buffered at pH 6.8, (monopotassium phosphate/di-sodium phosphate) using the rotating paddle method with a paddle rotating speed of 100 rpm (Type II paddle apparatus in accordance with the American Pharmacopeia USP 24).

[0154] The dissolution medium is continuously analysed by chromatography (HPLC) with UV detection. For each sample, measurement is performed on at least three vessels.

[0155] The results of the dissolution tests are summarized in FIG. 1.

[0156] Unexpectedly, it is observed that the tablets of the invention, even though they are insoluble, nevertheless have the capacity to release the active ingredient they contain over an extended period, i.e. over periods of more than 8 hours, preferably more than 12 hours, and further preferably more than 20 hours.

[0157] Said tablets are therefore of particular interest for the production of pharmaceutical forms of (Once-a-Day) type, i.e. only requiring one administering per day.

EXAMPLE 2

Manufacture of Tablets Containing Granules Obtained by Granulating Oxycodeine and 6.46% HPMC and Containing a Compression Matrix Consisting of a (1:1) Mixture of Two Excipients (Microcrystalline Cellulose and PVA/Povidone 80:20)

[0158] In this example, the applicant sought to determine the influence of the quantity of binder used during the granulation step on the dissolution profile of the tablets.

[0159] The granulation step is identical to the step described to produce tablets conforming to Example 1, with the sole exception that this time the quantity of binder (HPMC, Pharmacoat®606) is 6.46 weight % of the total weight of the granules. The composition of these granules is summarized in Table 6.

TABLE 6

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Percentage</th>
<th>Weight (g/batch)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Oxycodeine HCl</td>
<td>93.54</td>
<td>590.5</td>
</tr>
<tr>
<td>HPMC (Pharmacoat®606)</td>
<td>6.46</td>
<td>40.8</td>
</tr>
<tr>
<td>Purified water</td>
<td></td>
<td>483.9</td>
</tr>
<tr>
<td>Total (dry)</td>
<td>100.0</td>
<td>631.3</td>
</tr>
</tbody>
</table>

[0160] The mixing and compression steps are then conducted following exactly the same parameters as in Example 1, using the same qualitative and quantitative formula.

[0161] The characteristics of the tablets obtained according to Example 2 are summarized in Table 7. The mean values correspond to the mean calculated per 10 or 20 tablets.

TABLE 7

<table>
<thead>
<tr>
<th>Weight (mg)</th>
<th>Shape</th>
<th>Size (mm)</th>
<th>Thickness (mm)</th>
<th>Hardness (Newton)</th>
<th>Crush resistance (MPa)</th>
<th>Friability (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>227.0</td>
<td>Oblong</td>
<td>11 x 5</td>
<td>4.2</td>
<td>397</td>
<td>6</td>
<td>0.0</td>
</tr>
</tbody>
</table>

[0162] The tablets obtained following Example 2 show very strong crush resistance, equal to 6 Mpa, and zero friability. No heating step before or during compression was necessary to obtain tablets of such hardness.

[0163] The dissolution profile of these tablets is then determined as described in Example 1. This profile is illustrated FIG. 2.

[0164] The quantity of binder used has little influence on the release kinetics which extend over 24 h.

EXAMPLE 3

Tablets Obtained According to Example 2, Film-Coated with an Outer Coating of Aquacoat® ECD-30 (Ethylcellulose)

[0165] In this example, an assessment is made of the influence of an outer coating applied to the oxycodeine tablets obtained following Example 2. Here again, no heating step was applied either to the mixture to be compressed or to the compression tooling, whether before or during the actual compression.

1. Preparation of the Tablets

[0166] 1.1. Sub-Coating

[0167] Prior to coating with the actual polymer, a sub-coating step is applied to the tablets obtained in Example 2.

[0168] This sub-coat is intended to improve the surface condition of the tablets. It consists of a mixture of HPMC (Pharmacoat®603), an anti-flooding agent (Simethicone, Dow Corning), a lubricant (miconised talc, Lusenac UniVar) and anti-static agent (Syloid 244, Keyser & McKay), the HPMC representing a weight gain of 3% relative to the total weight of the uncoated tablets. The proportions of each of the excipients are given in Table 8.

TABLE 8

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Percentage</th>
<th>Weight (g/tablet)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Tablets</td>
<td>95.96</td>
<td>1000.0</td>
</tr>
<tr>
<td>XCOX5111</td>
<td></td>
<td>227.0</td>
</tr>
<tr>
<td>HPMC (603)</td>
<td>2.88</td>
<td>30.0</td>
</tr>
<tr>
<td>Simethicone (dry weight)</td>
<td>0.01</td>
<td>0.1</td>
</tr>
<tr>
<td>Talc</td>
<td>0.86</td>
<td>9.0</td>
</tr>
<tr>
<td>Syloid®244</td>
<td>0.29</td>
<td>3.0</td>
</tr>
<tr>
<td>Purified water**</td>
<td>N/A</td>
<td>308.5</td>
</tr>
<tr>
<td>Total (dry)</td>
<td>100.0</td>
<td>1042.07</td>
</tr>
</tbody>
</table>

**Note: the water is removed during the process; N/A: Not Applicable
This sub-coating is performed in conventional manner in a perforated pan (Trislot).

The parameters for the coating process are summarized in Table 9.

<table>
<thead>
<tr>
<th>Input temperature (°C)</th>
<th>38</th>
</tr>
</thead>
<tbody>
<tr>
<td>Output temperature (°C)</td>
<td>32</td>
</tr>
<tr>
<td>Pan rotation speed (rpm)</td>
<td>15</td>
</tr>
<tr>
<td>Air flow rate (m³/h)</td>
<td>150</td>
</tr>
<tr>
<td>Spray pressure (MPa)</td>
<td>0.12</td>
</tr>
<tr>
<td>Spray rate (g/min)</td>
<td>2.0-2.6</td>
</tr>
</tbody>
</table>

Coating is conducted using an aqueous dispersion of ethylcellulose (Aquecoat® ECD-30, FMC) the proportion of ethylcellulose representing 2.87 weight % of the total weight of the coated tablets. The proportion of the different excipients is given in Table 10. Here again, no specific heating step of the tablets was performed, either before or during application of the sub-coat or the actual coating.

1.3. Curing Step

This is conducted in a perforated pan after coating, for 24 hours at 60°C to allow stabilization of the film coating.

The tablets undergo an extended curing step (3 months) at 40°C and 75% humidity to increase their hardness and to prevent their crushing by conventional techniques (under a lighter or spoon) but also by less conventional but more efficient techniques (mortar, pliers or hammer for example).

The tablets thus hardened have a hardness greater than 500 N, which is equivalent to a crush resistance of more than 7.4 MPa. Under these conditions, release of the active ingredient is maintained with more than 90% of active ingredient released over 24 h as illustrated FIG. 3.

4.1. Preparation of the Tablets

4.1.1. Preparation of the Compression Matrix

A pre-mixture of microcrystalline cellulose (Avicel® PH102, FMC) and precipitated silica (Syloid® 244, Keyser & Mc Kay) is formed in a cubic mixer (AR 401, Erweka) for 2 min at 40 rpm. The polyvinylacetate/povidone mixture (80:20) (Kollidon® SR, BASF) and the oxycodone granules are added to the previous pre-mixture and homogenization is conducted in a cubic mixer for 15 minutes at 40 rpm. Finally, the lubricant (magnesium stearate, Quimidis) intended to limit adherence and compression friction is added to the previous mixture according to the mixing parameters: 5 minutes at 40 rpm.

The quantity of granules used is determined so as to manufacture tablets containing 40 mg oxycodone.

The proportions of each of the excipients are summarized in Table 12 below.
4.1.2. Compression

[0184] The compression step of the final mixture obtained in the proceeding step is conducted on a compression press (PR-12, Svenic) under a compression force of 35 kN using oblong punches whose sizes are given in the table below.

[0185] Compression is performed in conventional manner without either the mixture to be compressed or the compression tooling being subjected to a heating step, whether before or during the actual compression step.

[0186] The tablets containing 40 mg oxycodone obtained after this step have the following characteristics which are given in Table 13:

<table>
<thead>
<tr>
<th>TABLE 13</th>
<th>Batch n° XCOXS112</th>
</tr>
</thead>
<tbody>
<tr>
<td>Weight (mg)</td>
<td>225</td>
</tr>
<tr>
<td>Size (mm)</td>
<td>11 x 5</td>
</tr>
<tr>
<td>Shape</td>
<td>oblong</td>
</tr>
<tr>
<td>Thickness (mm)</td>
<td>4.2</td>
</tr>
<tr>
<td>Surface area (mm²)</td>
<td>55</td>
</tr>
<tr>
<td>Hardness (N)</td>
<td>350</td>
</tr>
<tr>
<td>Crush resistance (MPa)</td>
<td>5.2</td>
</tr>
<tr>
<td>Friability (%)</td>
<td>0.0</td>
</tr>
</tbody>
</table>

[0187] It is therefore ascertained that the tablets conforming to the invention have very high crush resistance, of more than 5 MPa.

[0188] Other tablets containing a dose of 20, 40 and 80 mg are produced using a different process: the oxycodone granules are prepared in a high shear granulator. The mixture to be compressed is prepared as described for Examples 1 and 2. The tablets are compressed on a SVIAI PR12 rotary press, using oblong punches of different sizes depending on the doses to be manufactured, under a compression force in the order of 10 to 15 kN.

[0189] Their physical characteristics are given in Table 14 below:

<table>
<thead>
<tr>
<th>TABLE 14</th>
<th>Dose</th>
<th>Tablet weight</th>
<th>Size L x W x Thckn.</th>
<th>Hardness (Crush resistance)</th>
</tr>
</thead>
<tbody>
<tr>
<td>20 mg</td>
<td>175 mg</td>
<td>11.0 x 5.0 x 3.8 mm</td>
<td>300 N (4.9 MPa)</td>
<td></td>
</tr>
<tr>
<td>40 mg</td>
<td>225 mg</td>
<td>11.0 x 5.0 x 4.2 mm</td>
<td>350 N (5.2 MPa)</td>
<td></td>
</tr>
<tr>
<td>80 mg</td>
<td>325 mg</td>
<td>13.0 x 6.0 x 4.5 mm</td>
<td>400 N (5.6 MPa)</td>
<td></td>
</tr>
</tbody>
</table>

[0190] The tablets thus manufactured all have excellent crush resistance, which is greater than 6 MPa irrespective of their size, even though at no time during the process was it necessary to heat the constituents of the tablets or the compression tooling to increase their hardness and resistance.

[0191] The <b>Table</b> containing 40 mg of active ingredient after the compression step are then coated with a coating intended to delay their release profile into the body.

4.1.3. Coating

[0192] Coating of the tablets is conducted in a perforated pan (Trisol).

[0193] Coating uses an aqueous dispersion of ethylcellulose (Aquacoat® ECD-30, FMC) the proportion of ethylcellulose representing 2.87 weight % of the total weight of the coated tablets.

[0194] A curing step of the coating film is carried out in an oven at 60° C. for 24 h.

[0195] The proportion of the different excipients and the general formula of the coated tablets obtained are given in Table 15 below.

<table>
<thead>
<tr>
<th>TABLE 15</th>
<th>Batch n° XCOXS112</th>
</tr>
</thead>
<tbody>
<tr>
<td>Percentage</td>
<td>mg/tablet</td>
</tr>
<tr>
<td>Oxycodone (DV000165)</td>
<td>17.40</td>
</tr>
<tr>
<td>HPMC 606</td>
<td>1.20</td>
</tr>
<tr>
<td>Kollidon SR®</td>
<td>36.32</td>
</tr>
<tr>
<td>Avicel PH102</td>
<td>36.32</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>0.46</td>
</tr>
<tr>
<td>HPMC 603</td>
<td>2.76</td>
</tr>
<tr>
<td>Simethicone 30% (vs)</td>
<td>0.01</td>
</tr>
<tr>
<td>Aquacoat ECD-30 (vs)</td>
<td>2.87</td>
</tr>
<tr>
<td>DBS</td>
<td>0.69</td>
</tr>
<tr>
<td>Micronised talc</td>
<td>1.35</td>
</tr>
<tr>
<td>Syloid 244FP</td>
<td>0.63</td>
</tr>
<tr>
<td>Total</td>
<td>100.00</td>
</tr>
</tbody>
</table>

[0196] Other uncoated tablets containing doses of 20, 40, 80 and 160 mg are also coated following the method described above.

[0197] Their physical characteristics observed after coating are given in Table 16 below:

<table>
<thead>
<tr>
<th>TABLE 16</th>
<th>Dose</th>
<th>Tablet weight</th>
<th>Size L x W x Thckn.</th>
<th>Hardness (Crush resistance)</th>
</tr>
</thead>
<tbody>
<tr>
<td>20 mg</td>
<td>175 mg</td>
<td>11 x 5 x 3.8 mm</td>
<td>440 N (7.3 MPa)</td>
<td></td>
</tr>
<tr>
<td>40 mg</td>
<td>225 mg</td>
<td>11 x 5 x 4.2 mm</td>
<td>500 N (7.4 MPa)</td>
<td></td>
</tr>
<tr>
<td>80 mg</td>
<td>325 mg</td>
<td>13 x 6 x 4.5 mm</td>
<td>570 N (6.5 MPa)</td>
<td></td>
</tr>
<tr>
<td>160 mg</td>
<td>575 mg</td>
<td>15 x 7 x 5.8 mm</td>
<td>800 N (6.3 MPa)</td>
<td></td>
</tr>
</tbody>
</table>

[0198] The tablets thus manufactured all have excellent crush resistance, which is greater than 6 MPa irrespective of their size.

2. Dissolution Curves with and without the Presence of Alcohol in the Dissolution Medium

[0199] Coated 40 mg tablets prepared according to Example 4.3 are tested in dissolution under two conditions:

| 2000 | a) 0.1 N HCl medium without ethanol |
| 2001 | b) 0.1 N HCl medium with 40% ethanol |
| 2002 | Les dissolution conditions are as follows: rotating paddle method, paddle rotating speed: 100 rpm, volume of medium: 900 mL, 1 tablet per vessel. The oxycodone is assayed by 225 nm UV spectrophotometry. |
| 2003 | The results of the dissolution tests are given in FIG. 4. |
| 2004 | It is found that, despite the presence of alcohol in the dissolution medium, the tablets of the invention maintain a sustained-release dissolution profile. |

3. Dissolution Curves in Relation to pH

| 2005 | 40 mg tablets prepared as described above in this example were also tested with respect to pH independency i.e. their ability to maintain a constant release profile irrespective of the pH value of the dissolution medium. |
Two experimental conditions were used:
Dissolution medium of pH 6.8
Dissolution medium of pH 1.2

The dissolution profiles obtained are given in FIG. 5.

It is ascertained that irrespective of the acidity of the dissolution medium, the tablets conforming to the invention maintain a constant sustained-release profile.

These tablets can therefore be considered to be pH-independent, imparting thereto a particular advantage insofar as they can be used as vectors for any of type of active ingredient which is to be released over an extended time.

4.3. Stability Studies
4.3.1. Storage Stability

The coated tablets containing 40 mg oxycodone, obtained following the above-described method, are examined with regard to stability in order to determine their reaction to storage.

The tablets are stored for 6 months under accelerated stability conditions in accordance with ICH standards in force (45°C, 75% humidity) in two types of packs: a) Al/Al aluminum blister pack, and b) HDPE bottles (high density polyethylene) in the presence of a desiccant.

The characteristics of the tablets after the storage period are summarized in Table 17 below:

<table>
<thead>
<tr>
<th>Packaging</th>
<th>Initial dose</th>
<th>Dose after storage</th>
<th>Impurities</th>
<th>Hardness</th>
<th>Proportion of water</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blister</td>
<td>40 mg</td>
<td>40 mg</td>
<td>0.17%</td>
<td>&gt;500 N</td>
<td>3.5%</td>
</tr>
<tr>
<td>Al/Al</td>
<td>20 mg</td>
<td>20 mg</td>
<td>0.17%</td>
<td>440 N</td>
<td>3.5%</td>
</tr>
<tr>
<td>HDPE</td>
<td>20 mg</td>
<td>19.9 mg</td>
<td>0.17%</td>
<td>440 N</td>
<td>3.5%</td>
</tr>
<tr>
<td>HDPE</td>
<td>20 mg</td>
<td>19.9 mg</td>
<td>0.17%</td>
<td>440 N</td>
<td>3.5%</td>
</tr>
<tr>
<td>HDPE</td>
<td>20 mg</td>
<td>19.9 mg</td>
<td>0.17%</td>
<td>440 N</td>
<td>3.5%</td>
</tr>
</tbody>
</table>

4.3.2. Dissolution Profiles Obtained after a Storage Period

These dissolution profiles are obtained under the following conditions: rotating paddle method, paddle rotating speed: 100 rpm, volume of the dissolution medium: 900 mL., pH 6.8.

These are given in FIGS. 6 and 7.

It is found that not only is the quantity of active ingredient maintained over time, but also that the release profiles of the active ingredient and the extreme hardness of the tablets are maintained after a storage period of 6 months.

The tablets conforming to the invention are therefore stable and show a dissolution profile which is both pH-independent and independent of the presence (even strong presence) of alcohol in the dissolution medium.

4.4. Clinical Trials

The 40 mg tablets prepared in this example are also tested in vivo to determine the plasma profile of oxycodone in patients receiving said tablets.

A clinical trial (Algorithm, Canada, n= OXY/24018/8001) was conducted in 12 healthy, fasting, male and female volunteers separated into two semi-groups. Each semi-group was successively given the two treatments (tablets of the invention and reference product) after an intermediate period without any treatment (wash-out period).

The reference product used in this trial was OxyContin®, a sustained-release oxycodone tablet taken twice a day, also containing a dose of 40 mg. (batch N°121777, expiry date April 2007, Purdue).

The oxycodone plasma profiles obtained are given in FIG. 8 and the parameters are grouped together in following Tables 18 and 19:

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Mean</th>
<th>CV</th>
</tr>
</thead>
<tbody>
<tr>
<td>Cmax (mg/mL)</td>
<td>34.41</td>
<td>20.5</td>
</tr>
<tr>
<td>Tmax (hours)</td>
<td>10.01</td>
<td>16.6</td>
</tr>
<tr>
<td>AUC0-24 (mg/h/mL)</td>
<td>667.10</td>
<td>16.9</td>
</tr>
<tr>
<td>AUC0-24 (mg/h/mL)</td>
<td>679.84</td>
<td>17.1</td>
</tr>
<tr>
<td>AUC0-24 (%)</td>
<td>98.17</td>
<td>1.7</td>
</tr>
<tr>
<td>K12 (hours^-1)</td>
<td>0.1154</td>
<td>24.0</td>
</tr>
<tr>
<td>T1/2, 12 (hours)</td>
<td>6.39</td>
<td>28.0</td>
</tr>
</tbody>
</table>

Note: For Tmax values it is the mean value which is indicated;
CV: Coefficient of variation;
K12: elimination rate constant;
T1/2, 12: elimination half-life.

Therefore, the plasma profiles obtained show that there is no loss of bio-availability of the active ingredient, despite a decrease in Cmax.

As a result, these matrix tablets containing oxycodone conforming to the invention show a plasma profile after once-a-day administration in man such that the ratio of their Cmax to the Cmax observed after administration of OxyContin® extended release tablets having the same dosage, does not exceed 0.7.

Also, these matrix tablets containing oxycodone according to the invention have a plasma profile after once-a-day administration in man, such that the ratio of AUC0-24 observed with these tablets to the AUC0-24 value observed with OxyContin® extended release tablets having the same dosage, lies within the bioequivalence interval of 80 to 125%.

These results are particularly advantageous since they mean that the oxycodone is just as well absorbed by the body as the reference product but, since its maximum concentration is reduced by around 35% in the tablets of the invention, it affords a substantial reduction in the risks of adverse effects which occur with high plasma concentrations.

Example 5

Tablets of Oxycodeine and Naloxone

5.1. Preparation of the Tablets

Tablets conforming to the invention are prepared by associating two active ingredients: oxycodone and naloxone.

Naloxone is an opiate antagonist, which inhibits the activity of oxycodone if the tablet is tampered with for administration via injection. When the tablet is taken in usual man-
ner (oral route), the naloxone does not exert its antagonist effect since it is rapidly metabolised when ingested by oral route. The ratio of oxycodone/naloxone base used here is 4:1. [0227] The tablets are produced in the same manner as in Example 4 (granulation of oxycodone in a high shear granulator). They do not undergo any heat treatment either before, during or after compression.

[0228] The general formula of the tablets thus manufactured (batch XCOX 5723) is summarized in Table 20 below.

<table>
<thead>
<tr>
<th>Raw materials</th>
<th>Mg/tab</th>
<th>(%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Granulated oxycodone</td>
<td>22.66</td>
<td>12.51</td>
</tr>
<tr>
<td>Naloxone 2HCI(H2O)</td>
<td>6.10</td>
<td>3.37</td>
</tr>
<tr>
<td>Kollidon SR ®</td>
<td>75.54</td>
<td>41.71</td>
</tr>
<tr>
<td>Avicel PH102 ®</td>
<td>75.54</td>
<td>41.71</td>
</tr>
<tr>
<td>Syloid 244</td>
<td>0.367</td>
<td>0.20</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>0.91</td>
<td>0.50</td>
</tr>
<tr>
<td><strong>Total</strong></td>
<td><strong>181.1</strong></td>
<td><strong>100.0</strong></td>
</tr>
</tbody>
</table>

After compression the tablets have the physical characteristics given in following Table 21.

<table>
<thead>
<tr>
<th>Description of tablet</th>
<th>Round, flat, white</th>
</tr>
</thead>
<tbody>
<tr>
<td>Diameter</td>
<td>6 mm</td>
</tr>
<tr>
<td>Thickness</td>
<td>3.90 mm</td>
</tr>
<tr>
<td>Mean weight</td>
<td>175.8 mg</td>
</tr>
<tr>
<td>Hardness</td>
<td>31.5 N</td>
</tr>
<tr>
<td>Diametral resistance</td>
<td>8.6 Mpa</td>
</tr>
</tbody>
</table>

[0229] It is ascertained that, conforming to the invention, it is possible to produce tablets with very high crush resistance possibly containing two active ingredients, in particular one opioid agent and one antagonist agent blocking action of the latter in the event of administering of the tablet via intravenous route.

5.2. Dissolution Profiles

[0230] Dissolution tests are conducted, as in the preceding examples, under the following conditions: Type II paddle apparatus/100 rpm/medium pH 6.8/volume of dissolution medium: 900 mL/assay by continuous UV spectrophotometry at 225 nm/vessel width: 10 mm.

[0231] The profile is given FIG. 8.

[0232] It is found that these ultra-hard tablets show a sustained-release profile (90% of the active ingredient released after 12 hours).

**EXAMPLE 6**

**Tablets Containing Mineral Derivatives**

6.1. Preparation of the Tablets

[0233] The aim of this test is to produce tablets conforming to the invention in which mineral excipients are used as chief ingredient of the compression matrix.

[0234] Tablets are prepared containing oxycodone and dicalcium phosphate dihydrate (Emcompress®) to replace the excipients of Kollidon SR® and Avicel PH 102® type used in the preceding examples.

<table>
<thead>
<tr>
<th>Raw materials</th>
<th>Mg/tab</th>
<th>(%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Granulated oxycodone</td>
<td>22.57</td>
<td>12.90</td>
</tr>
<tr>
<td>Emcompress ®</td>
<td>151.21</td>
<td>86.40</td>
</tr>
<tr>
<td>Syloid 244FP</td>
<td>0.35</td>
<td>0.20</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>0.88</td>
<td>0.50</td>
</tr>
<tr>
<td><strong>Total</strong></td>
<td><strong>175.00</strong></td>
<td><strong>100.00</strong></td>
</tr>
</tbody>
</table>

[0237] The mixture obtained is compressed as in Example 1.

[0238] The physical characteristics of the tablets after compression are given in following Table 23:

<table>
<thead>
<tr>
<th>Description of tablet</th>
<th>Round, flat, white</th>
</tr>
</thead>
<tbody>
<tr>
<td>Diameter</td>
<td>6 mm</td>
</tr>
<tr>
<td>Thickness</td>
<td>3.16 mm</td>
</tr>
<tr>
<td>Mean weight</td>
<td>179.8 mg</td>
</tr>
<tr>
<td>Hardness</td>
<td>170 N</td>
</tr>
<tr>
<td>Diametral resistance</td>
<td>5.7 Mpa</td>
</tr>
</tbody>
</table>

[0239] It is ascertained once again that the crush resistance obtained is well above 4 Mpa, even though no heating step of the mixture or of the compression tooling was necessary.

6.2. Dissolution Profile

[0240] The tablets so obtained are then placed in a dissolution medium.

[0241] The dissolution conditions are the following: Type II paddle apparatus; paddle rotating speed: 100 rpm; medium pH 6.8; volume of dissolution medium: 900 ml; continuous UV at 225 mm; vessel 10 mm.

[0242] The results are given in FIG. 9.

[0243] It is found that the tablets conforming to the invention obtained using mineral excipients are able to release oxycodone over a relatively extended time period.

**EXAMPLE 8**

**Drug Abuse Tests**

8.1. Crush Tests

[0244] The objective of this example is to determine the difficulty in breaking or crushing and optionally obtaining a powder from the Oxycodone tablets conforming to the invention, compared with tablets of the reference oxycodone product (OxyContin®).

[0245] Four means were chosen to implement this step and placed in increasing order of difficulty:

- [0246] knife (Opinel® pocket knife type)
- [0247] coffee spoon
- [0248] combination pliers
- [0249] glass mortar and pestle (laboratory glassware)
Assessment of crushing difficulty was determined in relation to the hardness of the tablet. The physical characteristics of the tested OxyContin® tablets are given in Table 24.

<table>
<thead>
<tr>
<th>Tested tablet</th>
<th>Thickness (mm)</th>
<th>Diameter (mm)</th>
<th>Round pink</th>
<th>Oblique white</th>
<th>Wt. (mg)</th>
<th>Hardness (N)</th>
<th>Crush resistance (MPa)</th>
</tr>
</thead>
<tbody>
<tr>
<td>OxyContin®</td>
<td>3.43</td>
<td>7.24</td>
<td></td>
<td></td>
<td>135.9</td>
<td>105</td>
<td>2.7</td>
</tr>
<tr>
<td>Invention</td>
<td>3.30</td>
<td>11.0</td>
<td></td>
<td></td>
<td>175.9</td>
<td>467</td>
<td>8.8</td>
</tr>
</tbody>
</table>

The crush resistance of the reference tablets is 3.3 times less than that of the tablet conforming to the invention. The use of pliers allowed rough crushing of the tablets (pieces of 1 to 2 mm), both for the reference product and for the tablets of the invention.

After the rough crushing step using pliers, use of the laboratory mortar enabled a fine powder to be obtained in both cases. However, the use of the mortar on intact tablets conforming to the invention did not permit their crushing.

The crushing difficulty observed on each of the types of tablet in relation to the tool used is summarized in the following Table 25:

<table>
<thead>
<tr>
<th>Knife</th>
<th>Coffee spoon</th>
<th>Pliers</th>
<th>Mortar</th>
</tr>
</thead>
<tbody>
<tr>
<td>OxyContin®</td>
<td>Easy cut</td>
<td>Easy crushing</td>
<td>Very easy crushing</td>
</tr>
<tr>
<td>20 mg batch</td>
<td>Chipping</td>
<td>Easy cutting</td>
<td></td>
</tr>
<tr>
<td>Invention</td>
<td>Difficult cut</td>
<td>Crushing impossible</td>
<td>(without prior cutting)</td>
</tr>
<tr>
<td>20 mg</td>
<td>to cut no crushing</td>
<td>Easy crushing, chipping</td>
<td></td>
</tr>
</tbody>
</table>

The reference OxyContin® product can be crushed fairly easily, irrespective of the means used. Since it has low hardness strength, it has a tendency to chip.

On the other hand, the tablet conforming to the invention can only be crushed with combination pliers; a knife only achieves cutting but no crushing. After cutting, the pieces can be ground in a mortar.

8.2. Dissolution Tests

A tablet cut in half using a knife, and a tablet roughly crushed using pliers are subjected to a dissolution test to analyse the impact of cutting and crushing on the dissolution profile, compared with an intact tablet. This test is conducted on batch XCOX 5726 prepared following Example 4, and on the OxyContin® reference product.

The dissolution method is as follows: continuous dissolution, dissolution medium pH 6.8, 900 ml of medium per vessel, rotating paddle method, paddle rotating speed: 100 rpm, dosage: 40 mg active ingredient per vessel, vessel thickness: 10 mm; measurement by UV spectrometry (wave-length λ= 225 nm). Readings are taken every 5 minutes during the first hour, then every 15 minutes up to 24 hours.

The results obtained for dissolution in the pH 6.8 medium are given in following Table 26 and in FIG. 11.

<table>
<thead>
<tr>
<th>Time (h)</th>
<th>Whole tablet</th>
<th>Tablet cut in half</th>
<th>Tablet cut in pieces</th>
</tr>
</thead>
<tbody>
<tr>
<td>0.5</td>
<td>35.9</td>
<td>50.8</td>
<td>61.0</td>
</tr>
<tr>
<td>1</td>
<td>47.1</td>
<td>62.8</td>
<td>73.4</td>
</tr>
<tr>
<td>2</td>
<td>60.5</td>
<td>75.2</td>
<td>85.4</td>
</tr>
<tr>
<td>3</td>
<td>69.4</td>
<td>82.3</td>
<td>91.6</td>
</tr>
<tr>
<td>4</td>
<td>76.2</td>
<td>87.0</td>
<td>95.4</td>
</tr>
<tr>
<td>6</td>
<td>86.0</td>
<td>92.9</td>
<td>99.0</td>
</tr>
<tr>
<td>8</td>
<td>92.8</td>
<td>96.5</td>
<td>100.3</td>
</tr>
<tr>
<td>12</td>
<td>100.7</td>
<td>99.4</td>
<td>100.7</td>
</tr>
<tr>
<td>16</td>
<td>103.4</td>
<td>100.1</td>
<td>100.5</td>
</tr>
<tr>
<td>20</td>
<td>103.9</td>
<td>99.4</td>
<td>100.5</td>
</tr>
<tr>
<td>24</td>
<td>—</td>
<td>98.2</td>
<td>100.4</td>
</tr>
</tbody>
</table>

It is ascertained that in a pH 6.8 medium, the dissolution profile of the reference product is close to that targeted for the bare tablet i.e., without a sustained-release coating, whereas the profile of the tablet of the invention (<<QD>>), is close to that targeted for a sustained-release tablet.

The cutting in half of the tablet accelerates dissolution, and acceleration is increased when the tablet is cut in pieces for both types of tablets, making the active ingredient more rapidly available for absorption via oral route.

However, the profile of the oxycodone in the crushed <<QD>> tablet, conforming to the invention, remains a sustained-release profile.

8.3 Evaluation of Extraction of the Active Ingredient

The tested tablets are also evaluated regarding the extraction of their active ingredient for injection.

The applicant used the so-called <<Steribox®>> kit available in pharmacies and designed for drug addicts, for the purpose of preventing the transmission of pathogenic agents through the exchange of contaminated syringes.

The Steribox® contains:

- two 1 ml syringes,
- five 5 ml doses of water for injection preparations,
- two cups so-called Stericups®,
- two filters

Extraction of oxycodone from the reference product and from the tablet conforming to the invention is conducted as follows on each batch:

- 2 tests on a whole tablet,
- 2 tests on a tablet roughly crushed with pliers,
- 2 tests on a tablet of the invention crushed with pliers and then with mortar and pestle, and
- 2 tests on a reference tablet directly crushed in a mortar.

The tested extraction medium is the water supplied with the Steribox®, in the maximum available volume (2 ml).

The operating mode used for extraction is the one described in the leaflet supplied with the Steribox®:

1. Place the prepared sample (whole, roughly crushed or ground) in the cup.
2. Add 2 ml water using a gauged pipette,
9.1.1. Preparation of the Ingredients

The composition of the tablets is summarized in Table 28 below.

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Percentage [%]</th>
<th>Weight (mg/tablet)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Hydromorphone HCl</td>
<td>12</td>
<td>3</td>
</tr>
<tr>
<td>Kollidon SR</td>
<td>30</td>
<td>12.5</td>
</tr>
<tr>
<td>Avicel PH102</td>
<td>36</td>
<td>9</td>
</tr>
<tr>
<td>Silica</td>
<td>1</td>
<td>0.25</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>1</td>
<td>0.25</td>
</tr>
<tr>
<td>Total</td>
<td>100.00</td>
<td>25.00 mg</td>
</tr>
</tbody>
</table>

9.1.2. Compression

The hydromorphone is first mixed with the excipients forming the compression mixture (Avicel PH102, Kollidon® SR and silica) after a screening step intended to remove large-size particles and other aggregates. Mixing uses a dry process in a conventional blender (V Blender) for 20 minutes. The powdered magnesium stearate is then added to the mixture and the whole is again mixed for 2 to 5 minutes. Compression of the final mixture obtained is obtained by direct compression of the mixture on a 6-station, Swiec RT6 rotary press, using extra-deep concave punches 3 mm in diameter. The applied compression force is 17.8 KN.

9.1.3 Dissolution Profile

The dissolution profile of the tablets prepared in this manner is measured by 12-hour UV spectrophotometry under three conditions:

a) Without alcohol in 0.1 N HCl medium,
b) With 20% alcohol in 0.1 N HCl medium,
c) With 40% alcohol in 0.1 N HCl medium.

The dissolution conditions are as follows:
Type II paddle apparatus; paddle rotating speed: 100 rpm; volume of dissolution medium: 500 ml; 37° C; filter 45 μm, automatic sampling (closed circuit) at sampling times of 5, 15, 30, 45, 60, 120, 180 and 240 minutes. UV analysis at 280 nm with 1.0 cm cells; 10 tablets of hydromorphone are deposited in each vessel (equivalent to 30 mg/vessel).

Dissolution results are given in Fig. 12.

It is found that in all cases the tablets conforming to the invention show a sustained-release profile which is not modified through the presence of ethanol in the dissolution medium,
The hydromorphone tablets conforming to the invention therefore have both excellent crush resistance and good alcohol resistance. They are therefore fully suitable for active ingredients which may be subject to accidental misuse or to drug abuse.

**EXAMPLE 10**

**Tablets of Morphine Sulphate**

In this example, ultra-hard, non-coated tablets containing morphine sulphate are prepared, and their resistance to alcohol present in the dissolution medium is compared with that of a morphine sulphate formulation sold commercially under the trade name Avinza®. The tablets of the invention contain a dose of 30 mg.

10.1.1 Formulation

First microgranules of morphine sulphate are prepared by coating neutral particles of size 500 to 600 μm using a binding agent: HPMC.

These microgranules are then ground in a mortar to obtain a fine particle size allowing homogeneous mixing. The grindings are then mixed with the compression excipients to obtain the mixture which can be used to produce the ultra-hard tablets of the invention. The type and proportion of each excipient are summarized in Table 30.

**TABLE 30**

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Percentage [%]</th>
<th>Weight (mg/tablet)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Ground microgranules of morphine sulphate (batch NP062M82)</td>
<td>19.98</td>
<td>72.927</td>
</tr>
<tr>
<td>Kollidon® SR</td>
<td>39.74</td>
<td>145.05</td>
</tr>
<tr>
<td>Avicel® PH101</td>
<td>39.58</td>
<td>144.47</td>
</tr>
<tr>
<td>Syloid® 244</td>
<td>0.20</td>
<td>0.73</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>0.50</td>
<td>1.825</td>
</tr>
<tr>
<td>Total</td>
<td>100.00</td>
<td>365.00</td>
</tr>
</tbody>
</table>

10.1.2 Compression

Compression of the final mixture obtained is carried out on a tablet press (PR-12, Sviac) using round punches 10 mm in diameter and a compression force of 26.1 kN.

The characteristics of the tablets thus obtained are given in the following Table 31.

**TABLE 31**

<table>
<thead>
<tr>
<th>Batch number of tablets NP062M211C1</th>
<th></th>
</tr>
</thead>
<tbody>
<tr>
<td>Weight (mg)</td>
<td>365</td>
</tr>
<tr>
<td>Shape</td>
<td>Round and flat</td>
</tr>
<tr>
<td>Diameter (mm)</td>
<td>10</td>
</tr>
<tr>
<td>Thickness (mm)</td>
<td>3.7</td>
</tr>
<tr>
<td>Hardness (N)</td>
<td>&gt;343.23</td>
</tr>
<tr>
<td>Crush resistance (MPa)</td>
<td>&gt;5.9</td>
</tr>
<tr>
<td>Friability (%)</td>
<td>0.0</td>
</tr>
</tbody>
</table>

The hardness of the tablets obtained is greater than 343 N i.e. a crush resistance of more than 5.9 MPa and zero friability.

10.1.3 Dissolution Profiles

The dissolution profile of the tablets prepared according to the invention is measured by 12-hour UV spectrophotometry at pH 6.8 under three conditions:

- a) Without alcohol in the medium,
- b) With 20% alcohol in the medium,
- c) With 40% alcohol in the medium.

The dissolution conditions are as follows: rotating paddle apparatus; volume of dissolution medium: 500 mL; paddle rotating speed=100 rpm; one 30 mg tablet per vessel.

The dissolution results are shown FIG. 13.

It is found that in all cases the tablets conforming to the invention have a sustained-release profile which is not affected by the presence of ethanol in the dissolution medium. These tablets therefore have major resistance to alcohol, imparting a distinct advantage to the tablets of the invention over other commercially available, sustained-release morphine sulphate tablets.

Comparative dissolution tests were conducted on tablets prepared according to the invention and on commercially available morphine sulphate tablets (Avinza®). The dissolution method used was the same as the one described previously, with the sole exception that the dissolution medium is a 0.1N HCl medium. Two conditions were tested: 0.1 N HCl medium in the presence of 20% ethanol (A) and 0.1N HCl medium in the presence of 40% ethanol (B).

The dissolution results are shown FIG. 14.

The commercially available product shows a very rapid dissolution profile and is not a sustained-release form. Additionally, it has low alcohol tolerance since the dissolution rate increases with the quantity of alcohol present in the medium.

On the other hand, the dissolution rate of the tablet according to the invention is not modified by the presence of alcohol in the medium.

1. Water-insoluble, matrix tablets capable of releasing one or more active ingredients into the body over an extended time period and containing at least one active ingredient which may be subject to drug abuse dispersed within a compression matrix, said matrix comprising at least one excipient chosen from the group comprising sustained-release, pH-independent, water-insoluble polymers, mineral excipients and their mixtures, wherein the quantity of excipient and the compression conditions are chosen so that said tablets have a crush resistance of at least 4 MPa, advantageously at least 6 MPa.

2. Matrix tablets according to claim 1, wherein neither the mixture to be compressed, nor the compression tooling are subjected to a heating step either before or during the actual compression step.

3. Matrix tablets according to claim 1, wherein said compression matrix represents 50 to 98 weight % of the total weight of said tablet, advantageously 85 to 95%.

4. Matrix tablets according to claim 1, wherein said compression matrix comprises a mixture of at least two excipients chosen from the group consisting of sustained-release, pH-independent, water-insoluble polymers, mineral excipients and their mixtures.
5. Matrix tablets according to claim 1, wherein said sustained-release, pH-independent, water-insoluble polymers are chosen from the group consisting of cellulose derivatives, water-insoluble methacrylic acids, derivatives of polyvinylalcohols, derivatives of polyvinyl acetates, derivatives of polyvinylpyrrolidone, lactic and glycolic acid polymers, starches, waxes and their mixtures.

6. Matrix tablets according to claim 1, characterized in that the mineral excipients are chosen from the group consisting of calcium phosphates, aluminium and silicon silicates, magnesium carbonate and their mixtures.

7. Matrix tablets according to claim 1, wherein said polymers are chosen from the group consisting of microcrystalline cellulose and [polyvinyl acetate/polyvinylpyrrolidone (80:20)], and the mixture of microcrystalline cellulose and [poly(ethylacrylate/methylmethacrylate/trimethylammonioethyl methacrylate chloride)](1:2:0.2).

8. Matrix tablets according to claim 1, wherein said active ingredient(s) are chosen from the group consisting of psycho tropics, neuroleptics, tranquillizers, hypnotics, analgesics and anxiolytics.

9. Matrix tablets according to claim 1, wherein said active ingredients belong to the group consisting of morphine, oxycodone, hydrocodone, hydromorphone, oxymorphone, tramadol, methadone, codeine, fentanyl and buprenorphine, their salts and their pharmaceutically acceptable derivatives.

10. Matrix tablets according to claim 1, wherein said compression matrix also contains at least one pharmaceutically acceptable excipient chosen from the group consisting of anti-adherent agents, agents capable of improving tablet cohesion on compressing, fillers, lubricants, plasticizers, bulking agents, sweeteners and colouring agents.

11. Matrix tablets according to claim 1, wherein said compression matrix also comprises at least one or more of the following substances (a) to (f) or a mixture thereof:
   a) a substance which irritates the nasal and/or pharyngeal tracts,
   b) a viscosity-increasing agent, leading to formation of a gel when the tablet is dissolved in a minimum amount of water,
   c) an emetic substance,
   d) an averse colouring agent,
   e) a bitering substance,
   f) an antagonist of the active ingredient(s) which may be the subject of drug abuse.

12. Matrix tablets according to claim 11, wherein the antagonist agent of the said active ingredient(s) which may be the subject of drug abuse is naloxone or naltrexone or one of their pharmaceutically acceptable salts.

13. Matrix tablets according to claim 1, wherein said matrix tablets have an outer coating.

14. Matrix tablets according to claim 13, wherein said outer coating comprises of at least one sustained-release polymer advantageously chosen from the group comprising ethylecellulose derivatives and methacrylic polymers.

15. Matrix tablets according to claim 1, wherein said matrix comprises of a mixture of microcrystalline cellulose and [polyvinyl acetate/polyvinylpyrrolidone (80:20)] to the proportion of (1:1) and wherein said active ingredients which may be given drug abuse belong to the group of analgesics.

16. Matrix tablets according to claim 15, wherein said matrix tablets have an outer coating consisting of ethylecellulose.

17. Matrix tablets according to claim 1, wherein said matrix tablets are capable of releasing the active ingredient which may be subject to drug abuse over a period of more than 12 hours.

18. Matrix tablets according to claim 1, wherein said matrix tablets are capable of releasing the active ingredient which may be subject to drug abuse over a period of more than 20 hours.

19. Matrix tablets containing oxycodone according to claim 15, wherein said matrix tablets have a plasma profile after once-a-day administration in man, such that the ratio of the Cmax observed after administration of said tablets to the Cmax value observed after administration of OxyContin® extended release tablets containing the same dose, does not exceed 0.7.

20. Matrix tablets containing oxycodone according to claim 1, wherein said plasma profile after once-a-day administration in man is such that the ratio of AUC<sub>∞</sub> observed for said tablets to the AUC<sub>∞</sub> value observed with OxyContin® extended release tablets containing the same dose, lies in the interval of 80 to 125%.

21. Tablets according to claim 1, wherein said tablets can be administered once a day.

22. Method to produce matrix tablets according to claim 1, comprising the following steps:
   a) mixing the active ingredient(s) with the excipient(s) of the compression matrix,
   b) optional granulation,
   c) compression or mixing said mixture under conditions chosen so that said tablet has a crush resistance of at least 4 MPa, advantageously at least 6 MPa.

23. Method according to claim 22, wherein the compression step is conducted without the compression mixture or the compression tooling being subjected to a heating step either before or during the actual compression step.

24. Method according to claim 22, further comprising a coating step of said matrix tablet.

25. Method according to claim 24, further comprising a curing step of said outer coating.

26. A method, comprising administering a pharmaceutical composition in the form of tablets according to claim 1, for the sustained delivery of active ingredients which may be the subject of the drug abuse, intended to prevent the accidental misuse and/or to deter drug abuse of these active ingredients.

* * * * *