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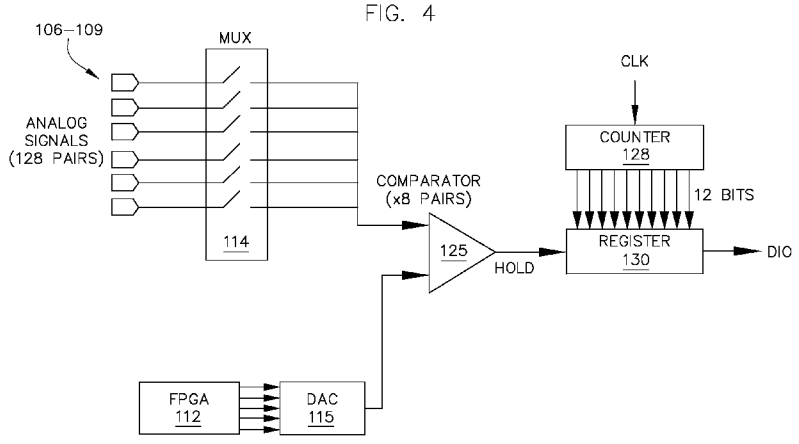
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(54) **Title**: APPARATUS AND METHOD FOR CHANNEL-SPECIFIC CONFIGURATION IN A READOUT ASIC

FIG. 4



(57) **Abstract**: An application-specific integrated circuit (ASIC) comprising a plurality of channels, each channel having circuitry for time and energy discrimination, a plurality of programmable registers, each programmable register configured to output at least one configuration parameter for the circuitry, and a channel-select register configured to identify a channel of the plurality of channels to be configured. The ASIC further includes a configuration-select register configured to identify the programmable register to be used for channel configuration, and a communications interface configured to transmit instructions received from a controller to one of the channel-select register, the configuration-select register, and the plurality of programmable registers.

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APPARATUS AND METHOD FOR CHANNEL-SPECIFIC CONFIGURATION IN A READOUT ASIC

CROSS-REFERENCE TO RELATED APPLICATION

[0001] This application claims the benefit of prior U.S. Provisional Application Serial No. 60/978,283 filed October 8, 2007, and which is incorporated herein in its entirety by reference.

GOVERNMENT RIGHTS NOTICE

[0002] This invention was made with government support under grant number HSHQDC-06-C-00089 awarded by the US Dept of Homeland Security. The government has certain rights in the invention.

BACKGROUND OF THE INVENTION

[0003] Embodiments of the invention relate generally to radiation detectors and, more particularly, to an apparatus and method for acquiring and processing electronic data from a radiation detector.

[0004] In the fields of security screening and medical imaging, non-invasive imaging techniques employing radiation detectors have gained importance due to benefits that include unobtrusiveness, ease, and speed. A number of non-invasive imaging techniques exist today. Single-photon-emission computed tomography (SPECT) imaging and x-ray computed tomography (CT) imaging are two examples.

[0005] At least two factors explain the increased importance of radiation detectors in security screening: an increase in terrorist activity in recent years, and an increase in the number of travelers. The detection of contraband, such as explosives and radioactive materials, being transported in luggage, cargo containers, and small vehicles and taken onto various means of transportation has become increasingly important. To meet the increased need for such detection, advanced systems have been developed that can not only detect suspicious articles being carried in luggage and other containers but can also determine whether or not the articles contain explosives or radioactive materials.

[0006] There is also a need for high-resolution gamma radiation detectors which can detect radioactive materials from a variety of sources. To gain widespread use, these radiation detectors must be economical, easily portable, and have low-power consumption. Semiconductor materials, such as cadmium-telluride (CdTe) and cadmium-zinc-telluride (CZT) crystals have applicability for compact radiation detectors. CdTe and CZT detectors have been shown to exhibit good energy resolution, especially as compared to scintillator-based detectors. Since they are direct conversion devices (i.e., convert radioactive particles, such as photons, directly into electronic signals), CdTe and CZT detectors eliminate the need for bulky photomultiplier tubes. Furthermore, CdTe and CZT radiation detectors do not require cryogenic cooling, as do high-purity germanium radiation detectors.

[0007] SPECT and CT imaging systems can incorporate such semiconductor, or solid state, radiation detector technology. CT systems are capable of acquiring mass and density information (as well as materials-specific information, such as an effective atomic number) on items within a piece of luggage. Although object density is an important quantity, surrogates such as "CT number" or "CT value" which represent a linear transformation of the density data, may be used as the quantity indicative of a threat. Features such as mass, density, and effective atomic number embody derived quantities such as statistical moments, texture, etc. of such quantities.

[0008] In CT imaging systems, an x-ray source emits a fan-shaped beam towards a subject or an object, such as, for example, a patient or piece of luggage. Hereinafter, the terms “subject” and “object” shall include anything capable of being imaged. The beam, after being attenuated by the object, impinges upon an array of radiation detectors. The intensity of the attenuated beam radiation received at the detector array is typically dependent upon the attenuation of the x-ray beam by the object. Each detector element of the detector array produces a separate electrical signal indicative of the strength of the attenuated beam received by each detector element. The electrical signals are transmitted from the detector array to a data processing system for analysis which ultimately produces an image.

[0009] Typically, in SPECT imaging systems, a gamma camera or similar radiation detector locates radiation emitted from a subject such as a patient, or an object such as a piece of luggage containing a radioactive substance. As above, "subject" and "object" are used interchangeably. When imaging a patient, a gamma-ray-emitting tracer material is administered to the patient. Typically, the tracer material is absorbed by the organ of interest to a greater degree than by other organs. In these systems, each element of the detector array produces a signal in relation to the localized intensity of the radiation emitted from the object. As with conventional x-ray imaging, the strength of the emission signal is attenuated by the inter-lying object or body part. Each element of the detector array produces a separate electrical signal indicative of the photon impinging upon the detector element. The electrical signals are transmitted from the detector assembly to a data processing system for analysis, which ultimately produces an image.

[0010] In SPECT imaging, a plurality of images is acquired at various angles around the area of interest. To acquire the images, the gamma camera is rotated around the patient. Generally, in transaxial tomography, a series of 2-D images, or views, are taken at equal angular increments around the patient. Typically, projections are acquired every 3-6 degrees. In some cases, a full 360 degree rotation is used to obtain an optimal reconstruction. Multi-head gamma cameras can provide accelerated image acquisition. For example, a dual-head camera can be used with detectors spaced 180 degrees apart, allowing two projections to be acquired simultaneously, with each head requiring 180 degrees of rotation. Triple-head cameras with 120 degree spacing are also used.

[0011] The series of views around the patient are reconstructed to form transaxial slices, or slices across the axis of rotation. The reconstruction is performed by a computer, which applies a tomographic reconstruction algorithm to the multiple views, yielding a 3-D dataset. This dataset may then be manipulated to show thin slices along any chosen axis of the body, similar to those obtained from other tomographic techniques, such as CT and PET.

[0012] A gamma camera radiation detector assembly may employ a multi-channel collimator and gamma ray detector to convert energy from the gamma ray photon into an electrical signal, which can be interpreted to locate the position of the gamma ray interaction in a planar detector. Gamma cameras may also include a large scintillation crystal responsive to radiation stimuli, such as gamma rays, emitted by the patient, and an array of photomultiplier tubes optically coupled to the crystal. In operation, the gamma rays emitted by the patient in the direction of the detector are collimated onto the crystal. Each gamma ray photon cloud that interacts with the crystal produces multiple light events that are detected by the photomultipliers near the point of interaction. Each light event detected by the photomultipliers produces an electrical signal. The electrical signals from the photomultiplier array are combined to provide an estimate of the location of the gamma ray emission. Analog and digital processing of the signal results in the generation of an image from the acquired data.

[0013] However, gamma cameras may also employ semiconductor detector elements, such as cadmium-zinc-telluride (CZT) elements, to replace the scintillator/photomultiplier system. CZT detector elements convert the signal from gamma ray photons directly into an electronic signal. By eliminating the light conversion step needed in scintillator/photomultiplier cameras, a gamma camera using semiconductor radiation detectors may exhibit higher signal to noise ratio, and increased sensitivity which can result in greater energy level resolution and better imaging contrast resolution.

[0014] SPECT and CT imaging systems incorporating semiconductor detector array technology may be able to provide compositional analysis of tissue using spectroscopic x-ray imaging while improving overall image quality and reducing the x-ray dose to the patient. Recent advances in the development cadmium-zinc-telluride (CZT) detectors and other direct conversion (i.e. semiconductor) detectors have extended the application of such detectors to medical imaging (i.e., SPECT and CT systems), security screening, nuclear experimentation, as well as to oil exploration and mining. As these detectors find more uses, increasing demands are placed on the electronic components of the detectors. The front end readout electronics or data acquisition system for a CZT

detector is generally expected to exhibit low-noise, high linearity, wide dynamic range, and good drive capability. In addition to these requirements, portable systems may also demand data acquisition systems that are low-power, low-cost, with a high channel count.

[0015] Primarily, front end readout electronics capture two pieces of information from the radiation detector: the energy level of the radiation and the timing of the detection. While the energy level indicates the energy spectrum of the radiation, timing information is used to determine the depth of interaction so as to provide the full 3D position sensitivity needed for image reconstruction. There have been several application-specific integrated circuits (ASICs) developed to function as the front end readout electronics for radiation detectors. Typically, these ASICs have high power consumption and only provide analog outputs, making it necessary to provide an external digitizer typically at increased cost and decreased reliability. Additionally, some of these recently developed readout ASICs may offer incomplete information as to the energy level or timing of the detection.

[0016] It would be desirable to have a data acquisition system for radiation detectors that can operate at low power, with little noise, offer complete energy level and time discrimination capabilities, and provide digital outputs.

BRIEF DESCRIPTION OF THE INVENTION

[0017] According to one aspect of the invention, an application-specific integrated circuit (ASIC) comprising a plurality of channels, each channel having circuitry for time and energy discrimination, a plurality of programmable registers, each programmable register configured to output at least one configuration parameter for the circuitry, and a channel-select register configured to identify a channel of the plurality of channels to be configured. The ASIC further includes a configuration-select register configured to identify the programmable register to be used for channel configuration, and a communications interface configured to transmit instructions received from a controller to one of the channel-select register, the configuration-select register, and the plurality of programmable registers.

[0018] In accordance with another aspect of the invention, a method of manufacturing an ASIC that includes providing a plurality of channels, each channel having a time discrimination circuit and an energy discrimination circuit, configuring a plurality of programmable registers to provide configuration parameters, and configuring a configuration-select register to identify the programmable register to be used for channel configuration. The method further includes configuring a channel select register to identify the channel to be configured, and configuring the plurality of channels to individually receive configuration parameters based on the contents of the channel-select and configuration-select registers.

[0019] According to yet another aspect of the invention, a data acquisition system including a sensor array having a plurality of outputs, a controller, and an ASIC, wherein the ASIC comprises a plurality of channels configured to receive a plurality of signals from the sensor array outputs, a plurality of programmable registers, each programmable register configured to output at least one program parameter to the plurality of channels, and a channel-select register configured to identify a channel of the plurality of channels to be programmed. The ASIC further includes a configuration-select register configured to identify a programmable register of the plurality of programmable registers to be used for channel programming, and a communications interface configured to receive instructions from the controller and transmit those instructions to one of the channel-select register, the configuration-select register, and the plurality of programmable registers. Furthermore, the data acquisition system controller is configured to instruct the ASIC to uniquely program each of the plurality of channels.

These and other advantages and features will be more readily understood from the following detailed description of preferred embodiments of the invention that is provided in connection with the accompanying drawings.

BRIEF DESCRIPTION OF THE DRAWINGS

[0020] FIG. 1 is a pictorial view of a SPECT imaging system according to an embodiment of the invention.

[0021] FIG. 2 is a block diagram of the system illustrated in FIG. 1.

[0022] FIG. 3 is a block diagram of one embodiment of a data acquisition system for a semiconductor radiation detector useable in the system illustrated in FIG. 1.

[0023] FIG. 4 is a block diagram of an analog-to-digital converter circuit useable in the system illustrated in FIG. 3.

[0024] FIG. 5 is a block diagram of channel configuration registers useable in the system illustrated in FIG. 3.

[0025] FIG. 6 is a block diagram illustrating the interaction between programmable registers and analog channel circuitry.

[0026] FIG. 7 is a schematic diagram of a latch useable in the system illustrated in FIG. 3

[0027] FIG. 8 is a block diagram of an energy discriminating circuit useable in the system illustrated in FIG. 3.

[0028] FIG. 9 is a schematic diagram of a charge-sensitive amplifier circuit for use in the energy discriminating circuit illustrated in FIG. 8.

[0029] FIG. 10 is a block diagram of time discriminating circuit useable in the system illustrated in FIG. 3.

[0030] FIG. 11 is a schematic diagram of a leading edge discriminator circuit for use in the time discriminating circuit illustrated in FIG. 10.

[0031] FIG. 12 is a schematic diagram of a time-to-voltage converter circuit for use in the time discriminating circuit illustrated in FIG. 10.

[0032] FIG. 13 is an illustration of a timing diagram for lock-out logic useable in the system illustrated in FIG. 3.

[0033] FIG. 14 is a pictorial view of a CT system for use with a non-invasive package inspection system.

DETAILED DESCRIPTION OF EXEMPLARY EMBODIMENTS

[0034] The operating environment of the invention is described with respect to both computed tomography (CT), and single photon emission computed tomography (SPECT) imaging systems. However, it will be appreciated by those skilled in the art that the invention is equally applicable for use with other systems, such as portable radiation detectors, or in systems having sensor arrays other than radiation detectors. Moreover, embodiments of the invention will be described with respect to the detection and conversion of gamma ray radiation. However, one skilled in the art will further appreciate that aspects of the invention may be equally applicable to the detection and conversion of other high frequency electromagnetic energy.

[0035] Referring to FIG. 1, a single photon emission computed tomography (SPECT) imaging system 10 incorporating an embodiment of the invention is shown as including a gantry 12. Gantry 12 has a gamma ray detector 18 that detects photons from gamma rays emitted from the subject 22. Although the subject 22 is shown as a person, it is to be appreciated that the SPECT imaging system 10 may be configured for industrial applications such as inspection imaging, or to image items of interest from a security perspective, such as, for example, luggage or packages. Referring now to FIG. 2, detector assembly 18 is formed by a plurality of radiation detectors 20 and data acquisition systems (DAS) 32. The plurality of radiation detectors 20 sense the gamma-rays 16 that pass through a subject 22, and DAS 32 converts the data to digital signals for subsequent processing. Each detector 20 produces an analog electrical signal that represents the intensity of an impinging gamma ray photon cloud and hence the attenuated photon cloud as it passes through the subject 22.

[0036] During a scan, gantry 12 and the components mounted thereon rotate about a center of rotation 24. Rotation of gantry 12 is governed by a gantry motor controller 30 of SPECT system 10. Gantry motor controller 30 controls the rotational speed and position of gantry 12. An image reconstructor 34 receives sampled and digitized data

from DAS 32 and performs high speed reconstruction. The reconstructed image is applied as an input to a computer 36, which stores the image in a mass storage device 38.

[0037] Computer 36 also receives commands and scanning parameters from an operator via console 40 that has some form of operator interface, such as a keyboard, mouse, voice activated controller, or any other suitable input apparatus. An associated display 42 allows the operator to observe the reconstructed image and other data from computer 36. The operator supplied commands and parameters are used by computer 36 to provide control signals and information to DAS 32, and gantry motor controller 30. In addition, computer 36 operates a table motor controller 44 which controls a motorized table 46 to position subject 22 and gantry 12. Particularly, table 46 moves subjects 22 through a gantry opening 48 of FIG. 1 in whole or in part.

[0038] FIG. 3 shows a schematic block diagram of an electronic system 100 for the acquisition of data from a sensor array or a semiconductor, or solid state, radiation detector 105 such as a CZT detector, according to an embodiment of the invention. Electronic system 100 includes a low-noise, low-power, multi-channel readout ASIC 102 having one hundred and twenty-six anode channels 106, 108 and two cathode channels 107, 108. Each channel 106-109 has an energy discriminating circuit (discussed below with respect to FIG. 8) and a time discriminating circuit (discussed below with respect to FIG. 10). The ASIC 102 also has built-in analog to digital converters (ADCs) 110, or digitizers, to digitize the signal from energy sub-channels 200 in FIG. 8 and timing sub-channels 250 in FIG. 10. In one embodiment, ASIC 102 is fabricated using a CMOS process, achieving 20 nanosecond timing resolution while consuming less than 1 mW per channel and adding less than 4.5 keV (FWHM) equivalent noise at two picofarads parasitic capacitance to the anode energy reading. Electronic noise for cathode readings generally adds less than seven keV at ten picofarads parasitic capacitance.

[0039] The block diagram of FIG. 3 shows an embodiment of the front end readout electronics for data acquisition system 100 that could be used in conjunction with sensor

array or semiconductor radiation detector 105. One hundred twenty-four channels of the anode channels 106 are configured to interface with anodes (not shown) of detector 105, and cathode channel 107 is configured to interface with a cathode (not shown) of detector 105. There are two test channels 108 (one anode and one cathode) to facilitate stand-alone testing of ASIC 102. Tracker channel 109 is configured to monitor the variation of ASIC 102 parameters with environmental conditions and to provide calibration data for a digital controller 112.

[0040] Tracker channel 109 allows the DAS to compensate for the effects of temperature changes on ASIC 102 circuitry. Controller 112, which includes temperature tracking circuitry, sends a temperature-insensitive reference signal (e.g., a bandgap signal) to the input of all input channels 106-109. The energy and timing information associated with the reference signal is processed and digitized by the plurality of ADCs 110. Controller 112 tracks the variation in the digital output of the ASIC 102 from a reference signal output from channels 106-109 and generates correction coefficients. The correction coefficients may be then applied to subsequent digital outputs from channels 106-109 to eliminate or reduce temperature-induced error.

[0041] In the embodiment of FIG. 3, a field programmable gate array (FPGA) acts as digital controller 112. Controller 112 may be configured to minimize energy usage of the ASIC 102 by operating the ASIC 102 at a nominal frequency, for example, from one to two megahertz, before a signal is received from the radiation detector 105. While ASIC 102 is waiting for a signal from the radiation detector 105, controller 112 operates in a quiet mode during which it has little or no communication with ASIC 102. Quiet mode operation is employed to minimize any signal noise that might introduce error into the energy and timing measurements performed by ASIC 102. After a signal, such as a HIT signal, is indicating detected radiation is received by ASIC 102 from the detector, controller 112 goes into an active mode in which the ASIC clock frequency may increase from the nominal frequency to about twenty megahertz to minimize the time needed to generate a digital output. The period during which ASIC 102 generates a digital output is called "dead time" because the ASIC cannot process subsequent detector signals during this time. Speeding up the ASIC clock after a HIT signal

reduces dead time. In active mode, processing circuits (not shown) within controller 112 are enabled, and multiplexers 114 in ASIC 102 are directed to assign energy and timing signals from the anode channels 106 and cathode channel 107 to specific ADCs 110. Controller 112 then causes a digital-to-analog converter (DAC) 115 to generate an analog signal ramp, or reference signal, used to digitize the energy and timing signals. Following digitization, controller 112 initiates the generation of waveforms used to reset ASIC 102 to quiet mode in which ASIC 102 is ready to receive and process new signals from radiation detector 105 and in which the ASIC 102 clock frequency is once again set to the nominal frequency.

[0042] A single gamma ray may deposit energy into multiple detector channels. Radiation detected by the detector is commonly referred to as an "event." Typically, for any radiation event, each anode channel 106 that registers a signal raises a digital HIT flag, which is stored in a HIT register 120. The digital HIT flag triggers the time stamping circuitry to sample the event time, while the energy channel measures the level of the charge deposit. The hits recorded in the HIT register 120 are combined to output a control trigger, or event trigger 121, to controller 112. In an embodiment of the invention, HIT register 120 contains one-hundred twenty-eight bits, one bit for each ASIC 102 channel. Initially, the bits would be set to a state indicating no hits detected. Once radiation is detected on a particular channel, the corresponding bit in HIT register 120 would transition low to high, or high to low. By querying HIT register 120 and reading all one-hundred twenty-eight bits, controller 112 determines the number of hits detected and on which channel the hit occurred.

[0043] In operation, upon receipt of event trigger 121 from ASIC 102, controller 112 causes DAC 115 to generate a reference signal in the form of a signal ramp to begin data conversion, in which the analog energy level and timing information are digitized or converted to digital form. Event trigger 121 is de-asserted during digitization, and then re-asserted when digitization is complete. Re-assertion of event trigger 121 discontinues the ramp signal from DAC 115. Upon completion of digitization, controller 112 resets ASIC and de-asserts event trigger 121, readying ASIC 102 for the next event. The energy level information is preferably digitized with 12-bit resolution,

which corresponds to a 4.5 keV energy resolution, and the timing information is preferably digitized to 10-bit resolution, which corresponds to a five nanosecond timing resolution. Multiple ASICs 102 may be tied to a single controller 112 and DAC 115 to achieve higher channel counts. For example, controller 112 can also synchronize the HIT data from multiple ASICs 102 to determine the energy level and timing of coincident radiation events that are simultaneously detected on different ASICs 102.

[0044] Referring to FIG. 4, a schematic block diagram of an analog-to-digital converter is shown. The analog signal from a separate digital-to-analog conversion (DAC) 115 chip, controlled by digital controller 112, is used by an analog-to-digital converter (ADC) 110 in FIG. 3 circuit in ASIC 102 to generate the ASIC's digital output. The analog energy and timing signals from anode channels 106 and cathode channel 107 are routed to a pair of comparators 125 having two inputs. The inputs to one comparator include the output of the energy discriminating circuit and an output of DAC 115. The other comparator receives the output of the time discriminating circuit and an output of DAC 115. Controller 112 simultaneously starts a counter 128 and instructs DAC 115 to supply a signal ramp, or reference signal, to the pair of comparators 125. When the voltage from DAC 115 reference signal increases beyond the voltage of the energy signal on the comparator 125, it causes the comparator 125 output to trip, latching the counter 128 value at the time comparator 125 tripped into register 130. The value on counter 128 that is latched into register 130 upon comparator 125 tripping represents the digital value, or time stamp, of the analog energy signal. This process is repeated to obtain a digital value for the timing signal on the remaining comparator 125. The same reference signal may be used for the digitization of both energy and timing signals. Furthermore, if the system contains multiple ASICs 102 tied to a single controller 112, a common reference signal may be used to generate the digital outputs for all of the ASICs 102 tied to that controller 112.

[0045] The ASIC's built-in ADC 110 circuitry includes eight pairs of ramp-based comparators 125 as shown in FIG. 4. Each pair of comparators 125 process energy and time information from one channel. It is contemplated that one pair of comparators 125 may be dedicated to cathode channels 107, 108 and another pair of comparators 125

may be dedicated to tracker channel 109. When an anode channel 106 registers a hit, controller 112 reads the HIT register 120, assigns each hit channel to a comparator 125 pair, and controls digitization by initiating an analog ramp from DAC 115.

[0046] Referring to FIGS. 3 and 4, ASIC 102 includes a plurality of programmable registers 122. In one embodiment, there are two hundred and fifty-six programmable registers 122 on ASIC 102, sixty-eight of which are reserved for channel specific actions such as bus connect, channel enable/disable, and digital test bits. The remaining one hundred and eighty-eight programmable registers 122 are used for waveform generation, testing, and channel configuration.

[0047] Channel configuration involves setting of certain parameters for the energy and time discrimination circuits. Those parameters include the setting of low-trim threshold, power supply level, shaping time constant, and channel connection to the multiplexer 114. Configuring each anode channel 106 separately increases the effectiveness of ASIC 102 by accounting for variation in electronic device properties across different channels. The low-trim threshold refers to the anode channel signal threshold voltage above which the signal is considered a valid hit. Anode signals below the low-trim threshold are considered to be noise or digital crosstalk. Because the radiation detector 105 elements connected to anode channels 106 exhibit variable leakage currents, it is more effective to be able to set the low-trim threshold and leakage compensation separately for each anode channel 106.

[0048] FIG. 5 is a block diagram of channel configuration registers of ASIC 102 (shown in FIG. 3). In one embodiment, all one hundred and twenty-eight anode and cathode channels 106-109 can be configured using just three dedicated registers 132, 134. ASIC 102 includes two Configuration-Select registers 132 containing the location of one or more configuration registers configured to store the desired configuration parameters for the specific channel to be configured. Activate Channel Number register 134 contains the number of the channel to be configured. Using just three registers 132, 134 to configure all one hundred and twenty-eight anode and cathode channels simplifies the layout of ASIC 102 (in FIG. 3), especially when compared to readout

devices that use a separate configuration register for each anode and cathode channel. Also, having just three registers dedicated to channel-specific configuration and just eight ADCs (110 in FIG. 3) results in fewer digital signals to analog sections of ASIC 102 when compared to readout devices with one ADC for each channel and with more configuration registers. Fewer signals between digital and analog sections of the chip decreases the amount of analog-to-digital crosstalk and the resulting noise. The simplified layout of the registers on ASIC 102 permits registers 132, 134 that are used for channel configuration to be aligned with registers dedicated to each ASIC channel 106-109. As a result, digital signals to and from the ASIC's channel registers run substantially perpendicular to the ASIC's analog signals, further minimizing analog-to-digital crosstalk.

[0049] The impact of noise from digital lines on the more sensitive analog lines is reduced through the use of buffers 135 embedded in channel circuitry. When a digital signal is to be converted into an analog signal, the power for the signal transitions from a digital power supply domain to an analog power supply domain. Each of the buffers 135 includes an input that is referred to a digital power supply (not shown) and an output that is referred to an analog power supply (not shown). This allows the use of supplies having different voltage levels while reducing the impact of digital noise on analog lines.

[0050] A communications interface 136 facilitates communications between controller 112 (shown in FIG. 3) and the Active Channel Number register 134, the Configuration-Select register, and a plurality of programmable registers 304 (shown in FIG. 6 below). Communications interface 136 is configured to transmit the configuration parameters from controller 112 to the appropriate programmable register 304. Additionally, interface 136 transmits to the Configuration-Select register 132 data that includes the location of the specific programmable register 304 to be used for configuring, or programming, the designated analog circuit 302 (shown in FIG. 6 below) for the selected channel. Communications interface 136 also transmits data identifying the channel selected for programming to the channel-select register 134.

[0051] The block diagram of FIG. 6 illustrates an exemplary interaction map between programmable registers and the various elements of the ASIC channel circuitry according to an embodiment of the invention. A top row of the map includes the analog components 302 of the time and energy discrimination circuits (i.e., CSA, Shaper, Peak Detect, Leading Edge Discriminator, Hit Latch, Time-to-Voltage Converter, Multiplexer) specific to each channel. Each analog circuit block 302 has one or more blocks 303 beneath it with the programmable features of that circuit block 302. A plurality of programmable registers 304 set the programmable features 303 along the row corresponding to each programmable register 304. Each of the analog circuits 302 includes some channel-specific configuration to optimize the signal-to-noise ratio. Channel-specific configuration takes into account non-uniform detector characteristics such as leakage current, capacitor and resistor tolerances, random offset in the Leading Edge Discriminator 251 (shown in FIG. 8 below), and mismatch of current sources in the Time-to-Voltage Converter 258 (shown in FIG. 8 below).

[0052] Referring to FIGS. 6 and 7, channel-specific configuration is enabled via a plurality of low-noise latches 320 which are embedded in the analog circuitry of each ASIC channel. An output 322 of each latch 320 operates a switch, for example the ResetTVC switch 274 (shown in FIG. 12), which controls the analog characteristics that configure the channel. Data input lines 324 from configuration registers 304 to latch 320 typically run north to south on ASIC 102 (shown in FIG. 3). A channel-specific signal line 326 provides the signal to enable latch 320. Typically, analog signal lines run east to west on ASIC 102. For example, to test channel 39, a command is sent to the low-noise latch 320 in the CSA that controls testing. The ConfigData2 328 register in the digital portion of ASIC 102 is loaded with an AtestEnbl 329 bit set high. This sets the north-to-south data line for AtestEnbl 329 to high. Controller 112 (shown in FIG. 3) sends a command to the Activate Channel Number register 134 (shown in FIG. 5) in ASIC 102 with instructions to test channel 39 with the contents of ConfigData2 328. The ASIC, in turn, generates the enable signal Chan_Configdata2En 331 for channel 39.

[0053] As shown in FIG. 6, ConfigData2 328 is responsible for configuring the testing and disabling of channels. ConfigData2 328 also controls the multiplexer 114

(shown in FIG. 3) connecting the channel to the digitizer via a pair of MUX bits 332. Similarly, ConfigData1 333 is responsible for configuring Leakage Cnrl, Shaper Time Constant and TrimDAC. If a channel is to be tuned with respect to the ConfigData1 333 parameters, controller 112 (shown in FIG. 3) programs the ConfigData1 333 and Activate Channel Number registers 134. In response, ASIC 102 generates Chan_ConfigData1En 335 for the specified channel. Specific codes in the Activate Channel Number register 134 enable the programming of all channels from a single configuration register 304 or from all configuration registers 304. In this manner, all channels may have their baselines set before channel-specific configuration. In such a case, Chan_ConfigData1(2)En 331, 335 is simultaneously generated for all channels. Some digital signals 336 such as ResetCSA, AtestSample, and AtestHold that are generated by the Global Dynamic 337 configuration register are intended to be applied to all channels at once. Similarly, the Global Static 339 configuration register, which is used for product specific configuration, generates digital signals such as Cout and CFB 341 which configure all channels simultaneously.

[0054] FIG. 8 is a block diagram illustrating an embodiment of an energy discriminating circuit 200 for ASIC 102. The energy discriminating circuit 200 is designed to measure a charge created in detector 105 (shown in FIG. 3) by absorption of a gamma ray. Energy discriminating circuit 200 collects a charge, Q_{in}, from the detector 105 that is amplified by a charge sensitive amplifier 202. The signal from charge sensitive amplifier 202 is amplified again in an amplifier/buffer 203, which provides isolation and gain to the signal to facilitate further processing. The shape of the charge pulse from amplifier/buffer 203 is modified by a slow shaper 204 to improve the signal-to-noise ratio by limiting the bandwidth and increasing the duration of the pulse for the subsequent pulse peak detection. One embodiment of the invention uses a first order CR-RC pulse shaper 204 with a programmable shaping time from 500 nanoseconds to four microseconds. The gain of shaper 204 can also be programmed to one of four possible values.

[0055] The peak detect/hold (PDH) circuit 205 then detects and holds the peak of the pulse output from slow shaper 204 for digitization. PDH circuit 205 extracts the peak

value of the pulse and holds that peak value allowing for conversion of the analog signal to digital form. The peak detect signal is gated with a valid HIT signal. Without a valid HIT signal from the anode time discrimination circuitry, any peak detect signal would be ignored. The PDH circuit 205 also generates a digital peak-found signal when peak detect is complete to trigger an automatic transition from peak detect to peak hold mode.

[0056] In the embodiment of FIG. 9, a schematic diagram of charge sensitive amplifier (CSA) 202 of FIG. 8 is shown. CSA 202 integrates the charge Q_{in} collected by the detector 105 (shown in FIG. 3) and converts it to a voltage. Typically the signal Q_{in} from a semiconductor radiation detector 105, such as a CZT detector, is a quantity of charge delivered as a current pulse lasting from one nanosecond to ten microseconds, depending on the size and bias voltage of the detector. FIG. 9 illustrates one embodiment of CSA 202 that integrates charge on a feedback capacitor 210.

[0057] Another function of the CSA 202 is to minimize the amount of noise added to the signal. Typically, front end readout electronics for radiation detectors are generally expected to add no more than a few hundred electrons to the acquired signal. A continuous reset element 212, which is usually a resistive element, compensates for leakage current in DC-coupled detectors and prevents the CSA 202 from saturating. In an embodiment of the invention, anode leakage currents are typically about four-hundred fifty picoamps. For cathode channels, such as cathode channel 107 of FIG. 3, continuous reset element 212 may be eliminated since the signal Q_{in} from the cathode channel is preferably AC-coupled to ASIC 102 (shown in FIG. 3) through a capacitor (not shown). Cathode leakage currents may be, for example, on the order of forty-five nanoamps.

[0058] Referring to FIG. 10, a block diagram illustrating a time discriminating circuit 250 of ASIC 102 according to an embodiment of the invention is shown. Time discriminating circuit 250 serves two functions: to identify an event and raise a HIT flag, and to time stamp the event to within 20 nanoseconds FWHM (full width at half maximum). Thus, a single channel has two outputs: a digital HIT flag, and an analog

time stamp signal. Time discriminating circuit 250 includes a leading edge discriminator (LED) 251 that raises a HIT flag when a gamma ray is detected. LED 251 includes a fast CR shaper 252 and an LED comparator 254. One embodiment of the CR shaper 252 includes a programmable resistor array to optimize jitter, and four-bit programmable shaping times from twenty-five nanoseconds to four-hundred nanoseconds.

[0059] Referring again to FIG. 10, the leading edge discriminator 251 and latch 256 are followed by a time-to-voltage converter (TVC) 258 that provides a voltage proportional to the event time. TVC 258 has two inputs: the HIT signal from latch 256, and the TVCStop signal from controller 112. As will be explained more fully below, the TVCStop signal is generated based on the state of a clock signal from a clock signal generator (CSG) 257 in controller 112 and on the state of a lock-out signal from a lock-out signal generator 259 (LSG) in ASIC 102 (in FIG. 3) at the time the HIT signal occurred. TVC 258 produces an analog output voltage that is a linear function of the time at which the HIT signal occurred.

[0060] Referring to FIG. 10, a schematic diagram of the leading edge discriminator comparator 254 and latch 256, which raises the HIT flag described above. Other embodiments of the invention may use a constant fraction discriminator or a CR zero crossing discriminator. The three-stage comparator 254 of FIG. 10 provides an overall gain of about one thousand. Using three low-gain stages helps ensure linearity throughout the chain of amplifiers. NAND latch 256 provides a digital-compatible signal output. Typically, the baseline voltage is set close to mid-rail, and the threshold voltage is varied from 12 to 75 keV above the baseline voltage. In an embodiment of the invention, five bits are available to configure the threshold voltage. This configuration can be unique to a particular channel. The baseline and threshold voltages are reversed for the cathode channel 107 in FIG. 3.

[0061] FIG. 12 illustrates a schematic diagram of TVC 258 circuit realized as an integrator with a current source 266 that is turned on by the HIT signal from the timing circuit comparator 125 (shown in FIG. 4) and turned off by the closing of a TVCStop

switch 270. The signal to close TVCStop switch 270 is normally generated by controller 112 on the next rising edge of the ASIC clock, according to an embodiment of the invention. The integrator includes an operational transconductance amplifier (OTA) 280, a bank of feedback capacitors 276 and a series of switches. The voltage at a TVC output 272 is proportional to the time of integration, the constant of proportionality being the ratio of the integration current and the capacitance.

[0062] A reset switch 274 is used to initialize a TVC 258. Current source 266 is connected to capacitor bank 276 during the period of integration. At other times, current source 266 is sunk to a common-mode node 278 of operational transconductance amplifier (OTA) 280. As mentioned above, integration commences with the receipt of a control trigger signal 121 indicating a radiation event (shown in FIG. 3). Current source 266 is connected to the integrator thereby charging one or more capacitors in capacitor bank 276. The voltage on capacitor bank 276 continues to rise during integration. Controller 112 includes a clock generator which produces a system clock signal for all ASICs 102 coupled to controller 112. At the next rising edge of the ASIC system clock, current source 266 is switched from the integrator to common-node 278. The system maintains the voltage level on capacitor bank 276 at the value when current source 266 was disconnected. With reference to FIGS. 4 and 10, the capacitor bank 276 voltage is routed by multiplexer 114 routes to an input of one of the ASIC comparators 125. DAC 115 provides the second input to comparator 125. As explained above, when the reference signal from DAC 115 ramps up, controller 112 starts a counter 128. When the reference signal voltage reaches the capacitor bank 276 voltage, the comparator 125 output trips latching the counter 128 value into a register 130. The register 130 value is the time stamp for the detected radiation.

[0063] In an embodiment of the invention shown in FIG. 12, capacitance values for capacitor bank 276 typically range from 250 femtofarads to one picofarad. Switches Csel0, Csel1 on either side of capacitors C0, C1 allow capacitors C0, C1 to be connected or disconnected from the circuit as necessary. Programming of two bits controlling capacitor switches Csel0, Csel1 enables selection of four capacitor values.

As integration current is proportional to capacitance, the current has four possible values, typically ranging from 500 nanoamps to two microamps.

[0064] To prevent incomplete integration and reduce integral nonlinearity (INL) errors, there is a minimum integration time. As will be explained below, a lock-out signal generator 259 (in FIG. 10) in ASIC 102 (in FIG. 2) generates a lock-out signal, which is a phase-shifted version of the clock signal provided by controller 112, to ensure that the minimum integration time requirement is met. The integration is started asynchronously by the control trigger signal indicating a radiation event and is terminated by the TVCStop command, which is generated by controller 112 and can be initiated by the positive-going edge of an ASIC integration clock signal. In the absence of a lock-out signal, this maintains a maximum integration period of one microsecond (i.e., the period of one clock cycle), but can lead to arbitrarily short integration periods if the HIT signal occurs too close to the rising edge of the clock. In one embodiment of the ASIC 102 (shown in FIG. 3), in which the clock signal frequency is one megahertz, a TVC lock-out signal is used to keep integration times between 250 nanoseconds and 1.25 microseconds.

[0065] Referring to FIG. 13, a lock-out clock signal 282 is shown in quadrature with and leading an ASIC system clock signal, or integration clock signal 284. The phase shift between the integration clock signal 284 and the lock-out clock signal 282 represents the minimum integration time. For example, if the integration clock signal 284 and lock-out clock signal 282 have a one microsecond cycle time, the 90-degree phase shift illustrated in FIG. 13 translates into a 250 nanosecond minimum integration time. If an event 286 occurs before the rising edge of the lock-out clock signal 282, the integration continues until the next rising edge of the integration clock signal 284. This occurs irrespective of whether the event 286 occurs before or after the rising edge of the integration clock signal 284 and guarantees integration times between 250 nanoseconds and 750 nanoseconds, according to an embodiment of the invention. If the event 286 occurs after the rising edge of the lock-out clock signal 282, integration continues for an additional clock period ensuring a maximum integration time of 1.25 microseconds,

while avoiding integration periods of less than 250 nanoseconds, while and the associated integral nonlinearity (INL) errors.

[0066] A two-bit counter (not shown) is used to track the location of the event 286 edge with respect to the integration clock signal 284 and the lock-out clock signal 282. Events 286 get one of four clock stamps generated by the two-bit counter. The clock stamps are stored in a circular buffer. The relative position of all hits is determined by the digitized integration with, or time stamp value, and the clock stamp. The two-bit counter is synchronized across all ASICs in the system and with controller 112 (in FIG. 3), and can confirm the validity of the time stamp and provide controller 112 (in FIG. 3) with information on an integration width 288 so that, when needed, the additional clock period of integration may be subtracted from the event 286 time stamp. Controller 112 (shown in FIG. 3) coordinates the lock-out state across multiple ASICs 102 (shown in FIG. 3) to determine the coincidence of each event 286 registered.

[0067] Referring now to FIG. 14, package/baggage inspection system 500, incorporating embodiments of the invention, includes a rotatable gantry 502 having an opening 504 therein through which packages or pieces of baggage may pass. The rotatable gantry 502 houses a high-frequency electromagnetic energy source 506 as well as a detector assembly 508 semiconductor radiation detector elements, such as CZT detector elements similar to that shown in FIGS. 6 or 7. A conveyor system 510 is also provided and includes a conveyor belt 512 supported by structure 514 to automatically and continuously pass packages or baggage pieces 516 through opening 504 to be scanned. Objects 516 are fed through opening 504 by conveyor belt 512, imaging data is then acquired, and the conveyor belt 512 removes the packages 516 from opening 504 in a controlled and continuous manner. As a result, postal inspectors, baggage handlers, and other security personnel may non-invasively inspect the contents of packages 516 for explosives, knives, guns, contraband, etc.

[0068] Exemplary embodiments of the invention are disclosed with respect to use of the event timing circuit in a data acquisition system for radiation detectors. However, one skilled in the art will recognize that the invention is not limited to these

embodiments, and may also be employed in other applications in which it is advantageous to time stamp asynchronous events.

[0069] A technical contribution for the disclosed method and apparatus is that it provides for a controller implemented acquisition and processing of electronic data from a radiation detector.

[0070] According to one embodiment of the invention, an application-specific integrated circuit (ASIC) comprising a plurality of channels, each channel having circuitry for time and energy discrimination, a plurality of programmable registers, each programmable register configured to output at least one configuration parameter for the circuitry, and a channel-select register configured to identify a channel of the plurality of channels to be configured. The ASIC further includes a configuration-select register configured to identify the programmable register to be used for channel configuration, and a communications interface configured to transmit instructions received from a controller to one of the channel-select register, the configuration-select register, and the plurality of programmable registers.

[0071] In accordance with another embodiment of the invention, a method of manufacturing an ASIC that includes providing a plurality of channels, each channel having a time discrimination circuit and an energy discrimination circuit, configuring a plurality of programmable registers to provide configuration parameters, and configuring a configuration-select register to identify the programmable register to be used for channel configuration. The method further includes configuring a channel select register to identify the channel to be configured, and configuring the plurality of channels to individually receive configuration parameters based on the contents of the channel-select and configuration-select registers.

[0072] According to yet another embodiment of the invention, a data acquisition system including a sensor array having a plurality of outputs, a controller, and an ASIC, wherein the ASIC comprises a plurality of channels configured to receive a plurality of signals from the sensor array outputs, a plurality of programmable registers, each programmable register configured to output at least one program parameter to the

plurality of channels, and a channel-select register configured to identify a channel of the plurality of channels to be programmed. The ASIC further includes a configuration-select register configured to identify a programmable register of the plurality of programmable registers to be used for channel programming, and a communications interface configured to receive instructions from the controller and transmit those instructions to one of the channel-select register, the configuration-select register, and the plurality of programmable registers. Furthermore, the data acquisition system controller is configured to instruct the ASIC to uniquely program each of the plurality of channels.

[0073] While the invention has been described in detail in connection with only a limited number of embodiments, it should be readily understood that the invention is not limited to such disclosed embodiments. Rather, the invention can be modified to incorporate any number of variations, alterations, substitutions or equivalent arrangements not heretofore described, but which are commensurate with the spirit and scope of the invention. Additionally, while various embodiments of the invention have been described, it is to be understood that aspects of the invention may include only some of the described embodiments. Accordingly, the invention is not to be seen as limited by the foregoing description, but is only limited by the scope of the appended claims.

What is claimed as new and desired to be protected by Letters Patent of the United States is:

1. An ASIC comprising:

a plurality of channels, each channel having circuitry for time and energy discrimination;

a plurality of programmable registers, each programmable register configured to output at least one configuration parameter for the circuitry;

a channel-select register configured to identify a channel of the plurality of channels to be configured;

a configuration-select register configured to identify the programmable register to be used for channel configuration; and

a communications interface configured to transmit instructions received from a controller to one of the channel-select register, the configuration-select register, and the plurality of programmable registers.

2. The ASIC of claim 1, wherein the communications interface, in being configured to transmit instructions received from a controller, is configured to transmit configuration parameters from the controller to a selected programmable register of the plurality of programmable registers.

3. The ASIC of claim 2, wherein the communications interface, in being configured to transmit instructions received from a controller, is configured to transmit to the channel-select register a channel of the plurality of channels to be configured.

4. The ASIC of claim 3, wherein the communications interface, in being configured to transmit instructions received from a controller, is configured to transmit to the configuration-select register the location of a programmable register of the plurality of programmable registers to be used for channel-specific configuration.

5. The ASIC of claim 4, comprising a circuit configured to generate a channel-enable signal for the channel identified in the channel-select register to latch the contents of the programmable register to the channel circuitry being configured.

6. The ASIC of claim 1, wherein each channel comprises a plurality of latches configured to receive data from the programmable registers.

7. The ASIC of claim 6, wherein the plurality of programmable registers are aligned with the plurality of latches such that digital signal lines from the programmable registers run perpendicular to analog signal lines from the plurality of channels.

8. The ASIC of claim 6, wherein each latch is configured to output a signal to control a routing of configuration parameters.

9. The ASIC of claim 1, wherein each channel comprises a plurality of buffers, each buffer configured to accept a digital signal input and configured to produce an analog signal output.

10. A data acquisition system comprising:

a sensor array having a plurality of outputs;

a controller; and

an ASIC comprising;

a plurality of channels configured to receive a plurality of signals from the sensor array outputs;

a plurality of programmable registers, each programmable register configured to output at least one program parameter to the plurality of channels;

a channel-select register configured to identify a channel of the plurality of channels to be programmed;

a configuration-select register configured to identify a programmable register of the plurality of programmable registers to be used for channel programming; and

a communications interface configured to receive instructions from the controller and transmit those instructions to one of the channel-select register, the configuration-select register, and the plurality of programmable registers; and

wherein the controller is configured to instruct the ASIC to uniquely program each of the plurality of channels.

11. The system of claim 20, wherein the controller, in being configured to instruct the ASIC to uniquely program each of the plurality of channels, is configured to specify to the ASIC the channel of the plurality of channels to be programmed.

12. The system of claim 20, wherein the controller, in being configured to instruct the ASIC to uniquely program each of the plurality of channels, is configured to specify the programmable register of the plurality of programmable registers to be used for channel programming.

13. The system of claim 20, wherein the controller, in being configured to instruct the ASIC to uniquely program each of the plurality of channels, is configured to provide program parameters to the plurality of programmable registers.

FIG. 1

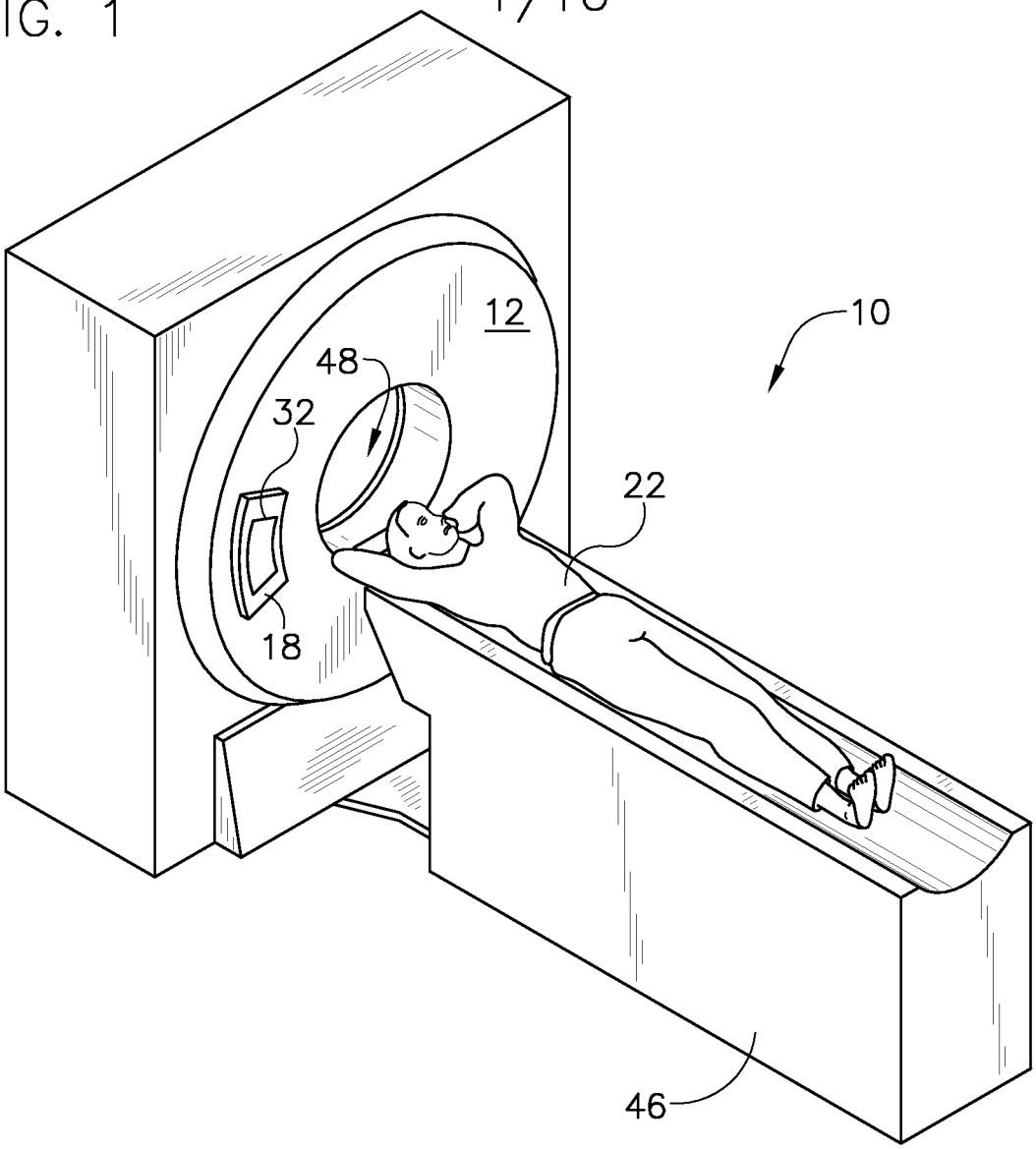
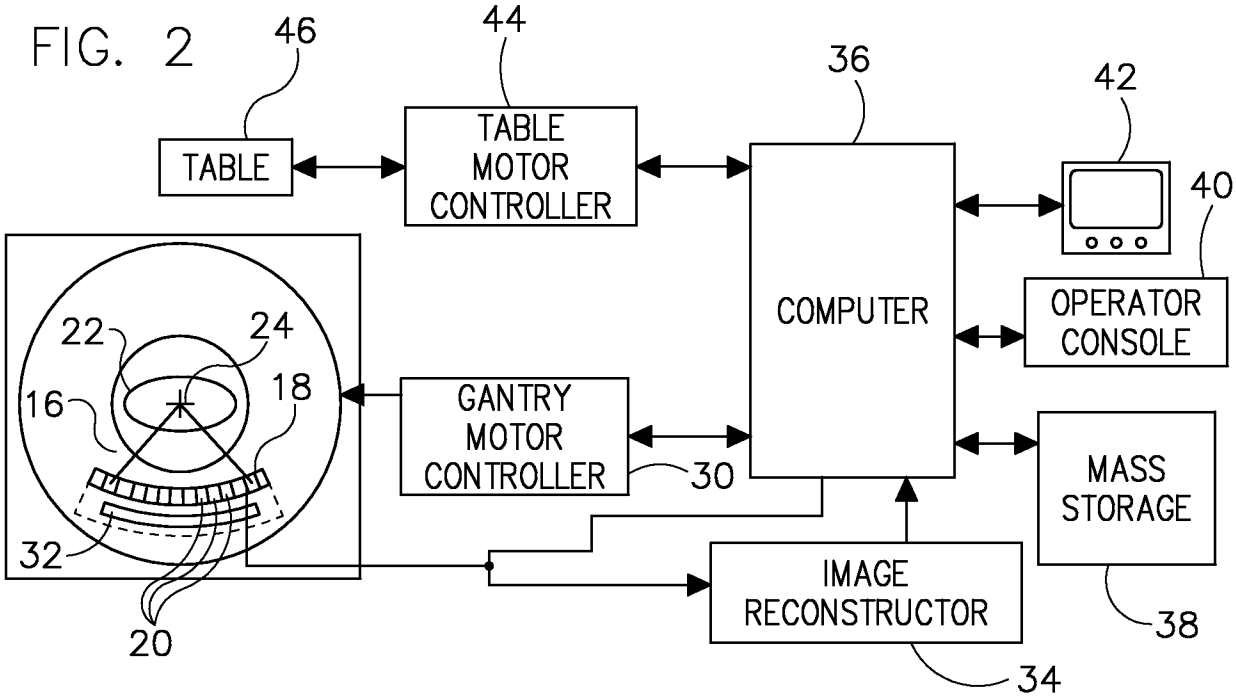

12
10
48
32
22
18
46

FIG. 2


46
44
36
42
TABLE
TABLE MOTOR CONTROLLER
40
COMPUTER
OPERATOR CONSOLE
22
24
16
18
GANTRY MOTOR CONTROLLER
30
MASS STORAGE
32
IMAGE RECONSTRUCTOR
38
20
34

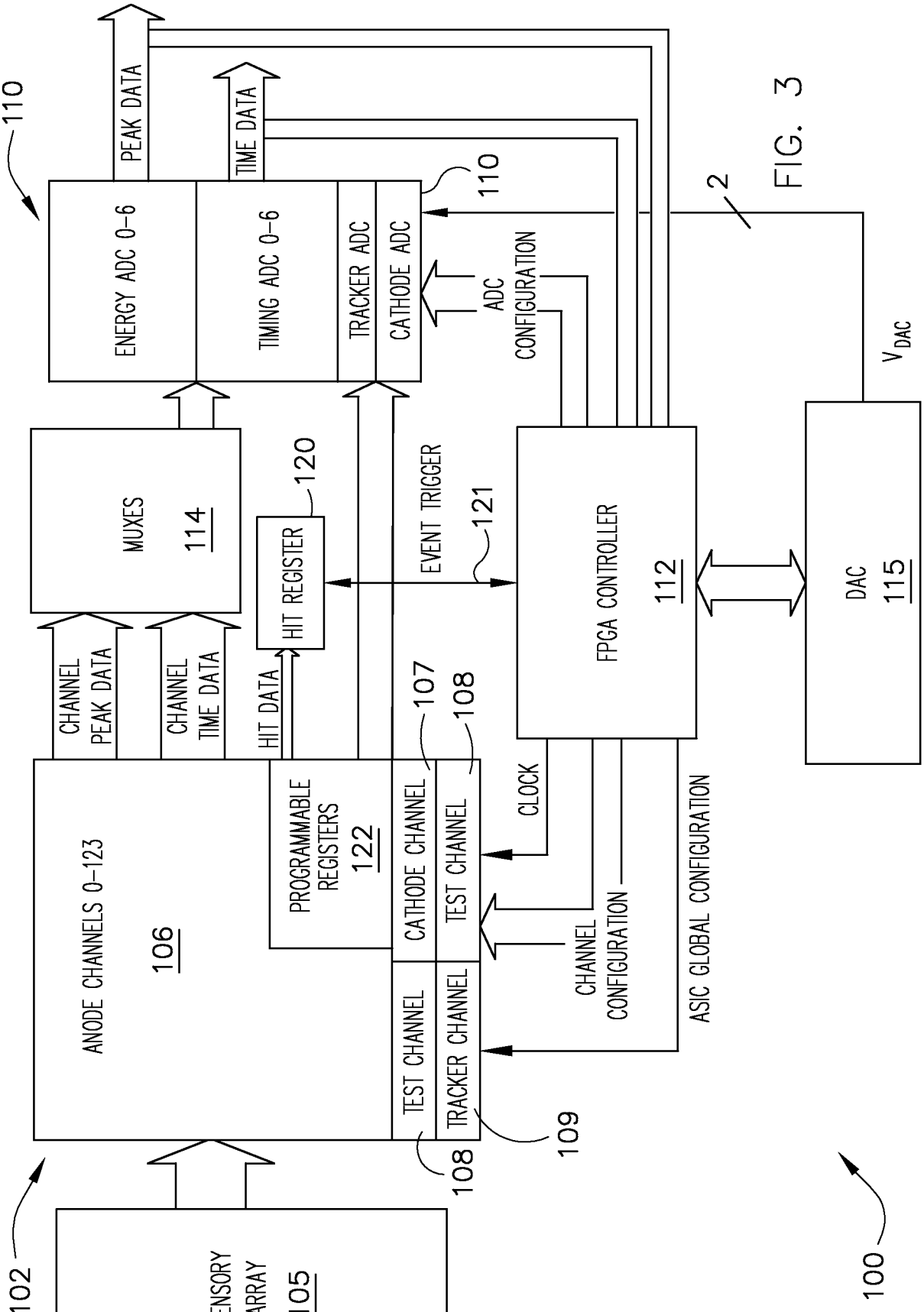

110
PEAK DATA
TIME DATA
ENERGY ADC 0-6
TIMING ADC 0-6
TRACKER ADC
CATHODE ADC
110
ADC CONFIGURATION
2
V_{DAC}
MUXES 114
120
HIT REGISTER
EVENT TRIGGER
121
FPGA CONTROLLER 112
DAC 115
CHANNEL PEAK DATA
CHANNEL TIME DATA
HIT DATA
107
108
PROGRAMMABLE REGISTERS 122
CATHODE CHANNEL
TEST CHANNEL
CLOCK
ANODE CHANNELS 0-123 106
CHANNEL CONFIGURATION
ASIC GLOBAL CONFIGURATION
TEST CHANNEL
TRACKER CHANNEL
108
109
SENSORY ARRAY 105
102
100

FIG. 3

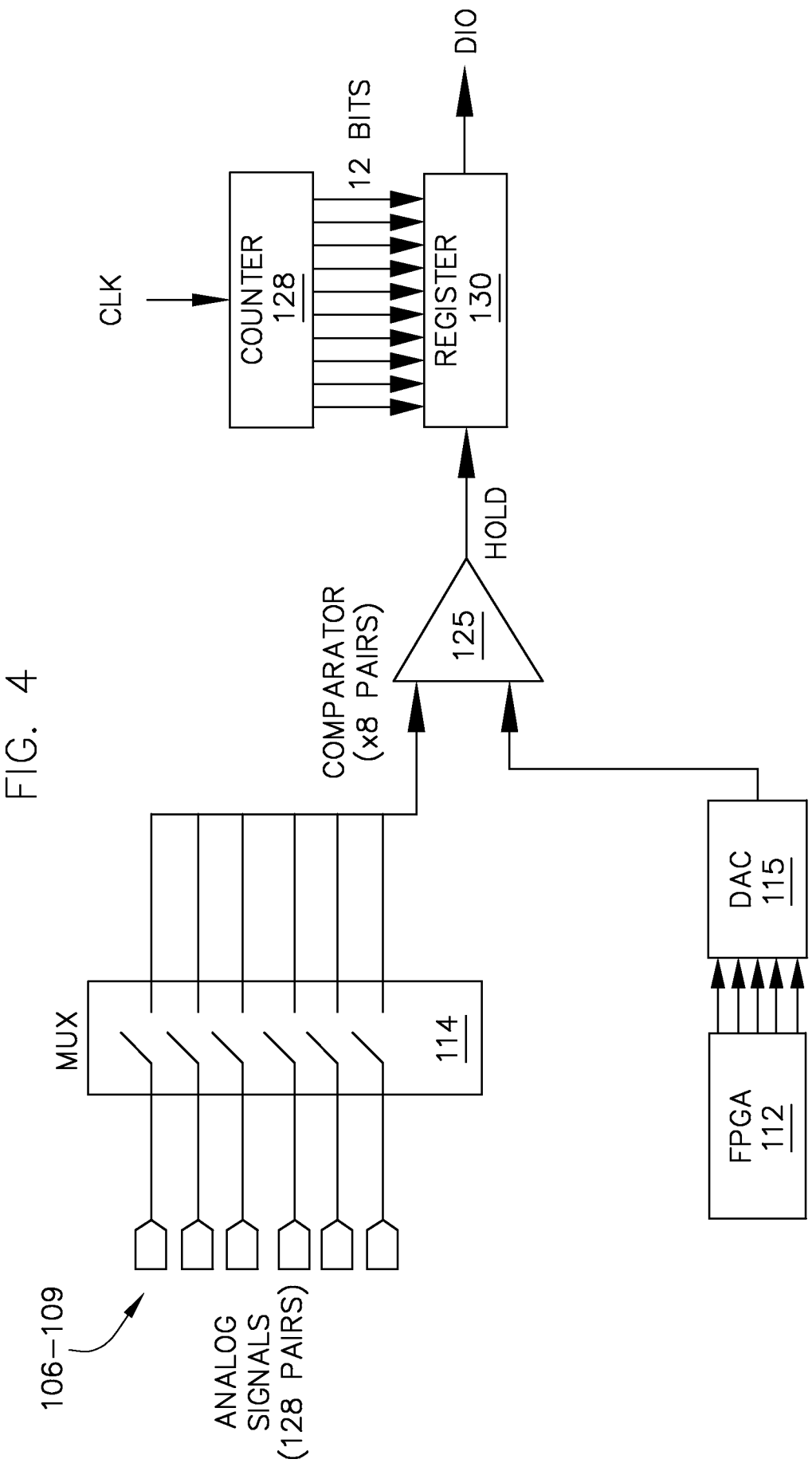

106–109
ANALOG SIGNALS (128 PAIRS)
MUX
114
COMPARATOR (x8 PAIRS)
125
HOLD
CLK
COUNTER 128
12 BITS
REGISTER 130
DIO
DAC 115
FPGA 112

FIG. 4

FIG. 5

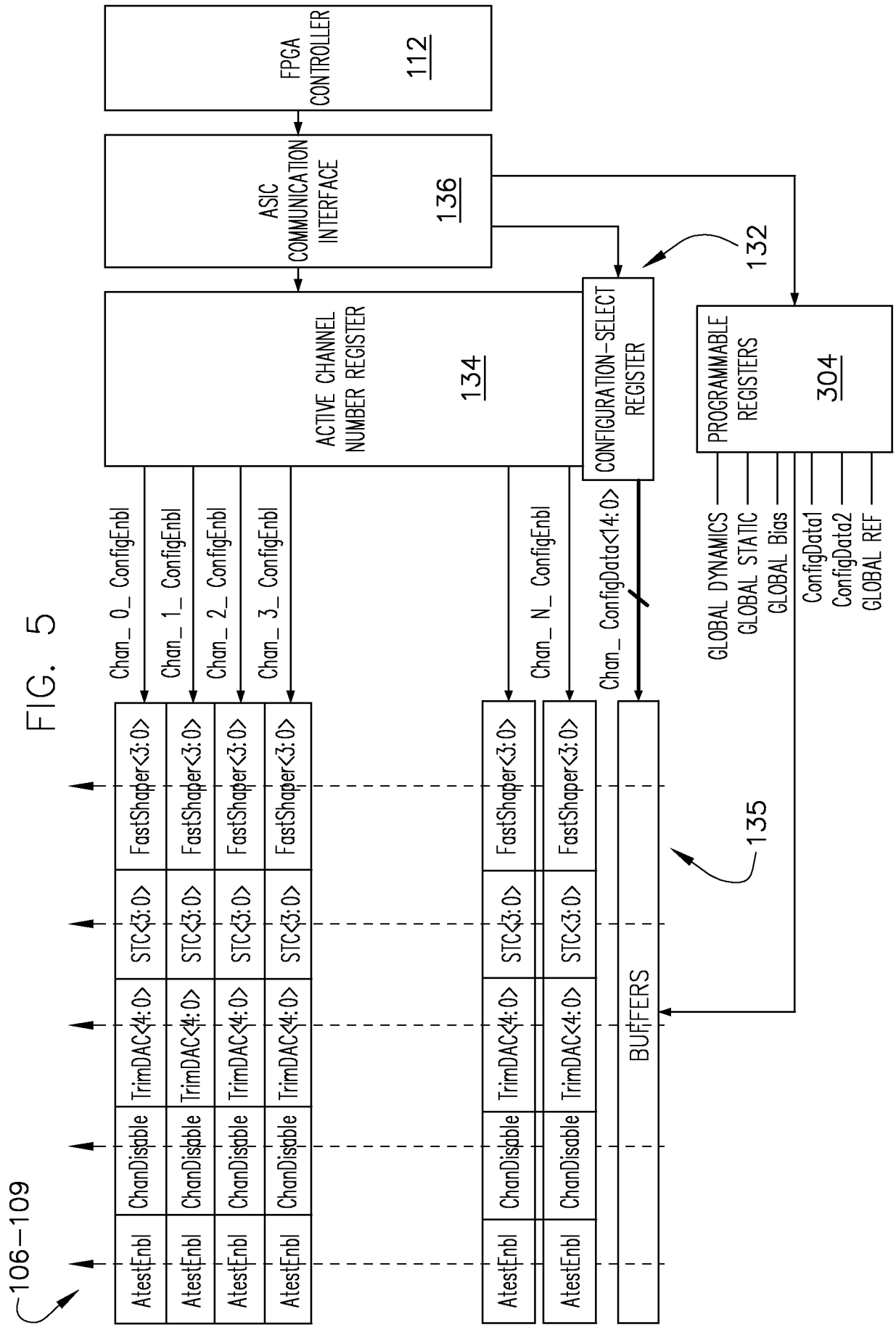

FPGA CONTROLLER
112
ASIC COMMUNICATION INTERFACE
136
ACTIVE CHANNEL NUMBER REGISTER
134
CONFIGURATION-SELECT REGISTER
132
PROGRAMMABLE REGISTERS
304
106-109
135
BUFFERS
Chan_ 0_ ConfigEnbl
Chan_ 1_ ConfigEnbl
Chan_ 2_ ConfigEnbl
Chan_ 3_ ConfigEnbl
Chan_ N_ ConfigEnbl
Chan_ ConfigData<14:0>
GLOBAL DYNAMICS
GLOBAL STATIC
GLOBAL Bias
ConfigData1
ConfigData2
GLOBAL REF
AtestEnbl
ChanDisable
TrimDAC<4:0>
STC<3:0>
FastShaper<3:0>

FIG. 6

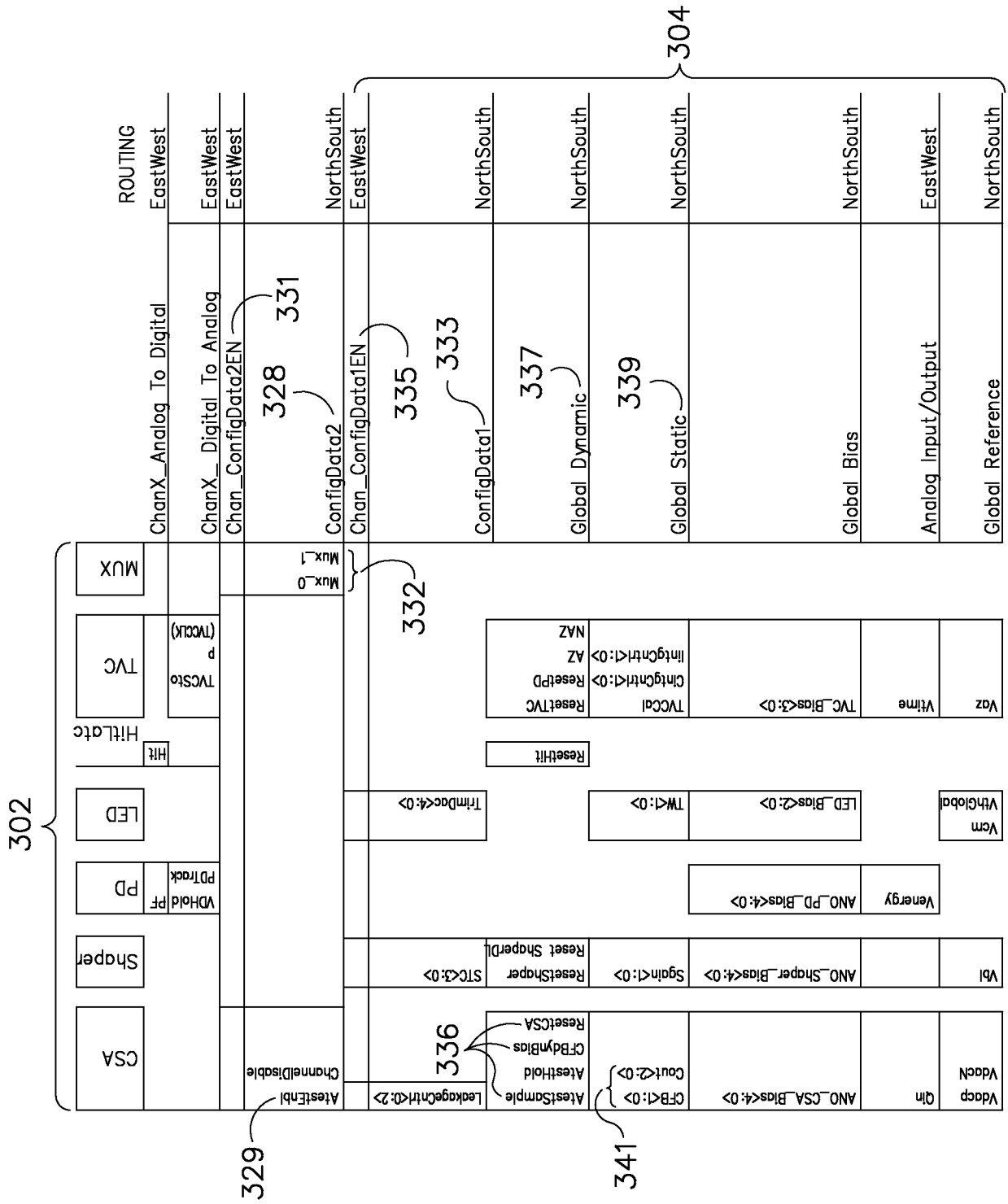

302
304
329
331
328
335
333
337
339
332
336
341
ROUTING
EastWest
ChanX_Analog_To_Digital
ChanX_ Digital To Analog
Chan_ConfigData2EN
ConfigData2
Chan_ConfigData1EN
ConfigData1
Global Dynamic
Global Static
Global Bias
Analog Input/Output
Global Reference
NorthSouth
EastWest
EastWest
NorthSouth
EastWest
NorthSouth
NorthSouth
NorthSouth
NorthSouth
EastWest
NorthSouth
MUX
TVC
HitLatc
LED
PD
Shaper
CSA
Mux_1
Mux_0
TVCSto
p
(TVCCLK)
Hit
VDHold
PDTrack
PF
AtestEnbl
ChannelDisable
LeakageCtrl<0:2>
AtestSample
AtestHold
CFBdyMBias
ResetCSA
CFB<1:0>
Cout<2:0>
ANO_CSA_Bias<4:0>
Qin
Vdacp
Vdacn
ResetShaper
Reset Shaperdl
STC<3:0>
SgainI<1:0>
ANO_Shaper_Bias<4:0>
Vbl
ResetHit
TrimDac<4:0>
TW<1:0>
LED_Bias<2:0>
Vcm
VthGlobal
ResetTVC
TVCCal
CintgCntrl<1:0>
IintgCntrl<1:0>
AZ
NAZ
TVC_Bias<3:0>
ANO_PD_Bias<4:0>
Venergy
Vtime
Vaz

FIG. 7

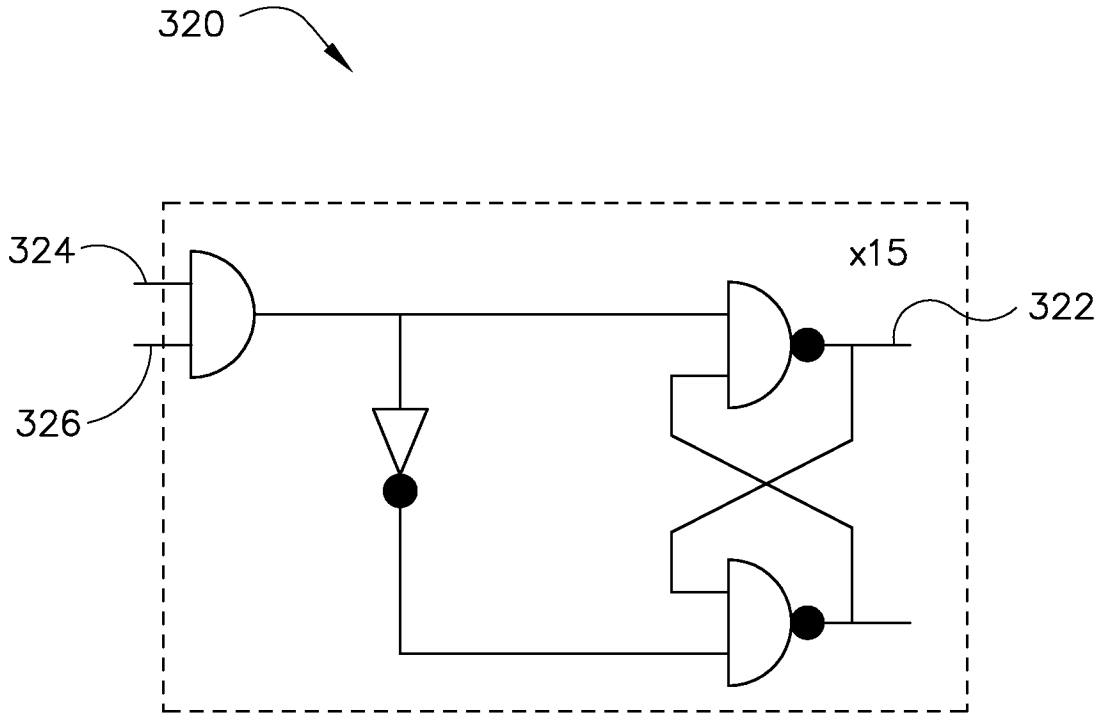


FIG. 8

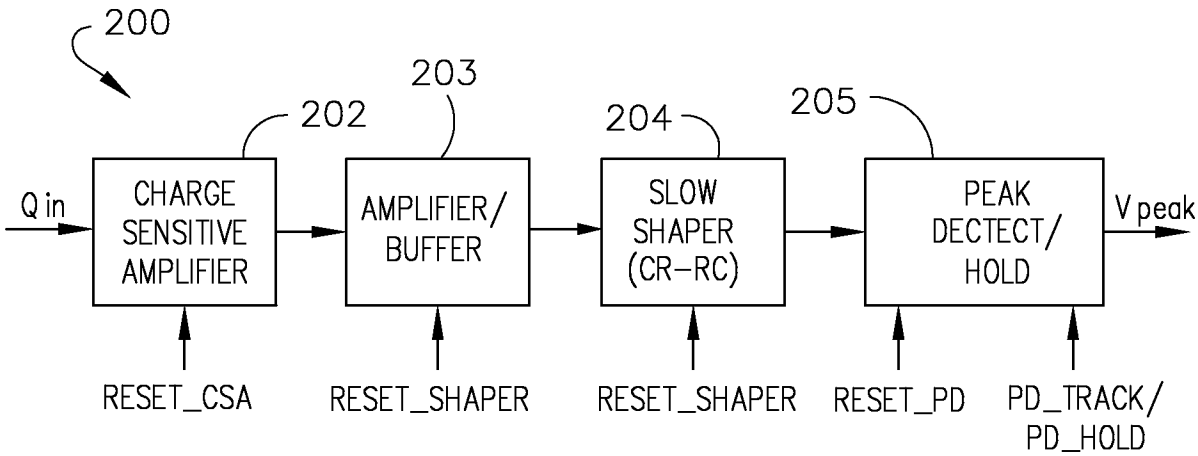

200
202
203
204
205
Q in
CHARGE SENSITIVE AMPLIFIER
AMPLIFIER/ BUFFER
SLOW SHAPER (CR-RC)
PEAK DECTECT/ HOLD
V peak
RESET_CSA
RESET_SHAPER
RESET_SHAPER
RESET_PD
PD_TRACK/ PD_HOLD

FIG. 9

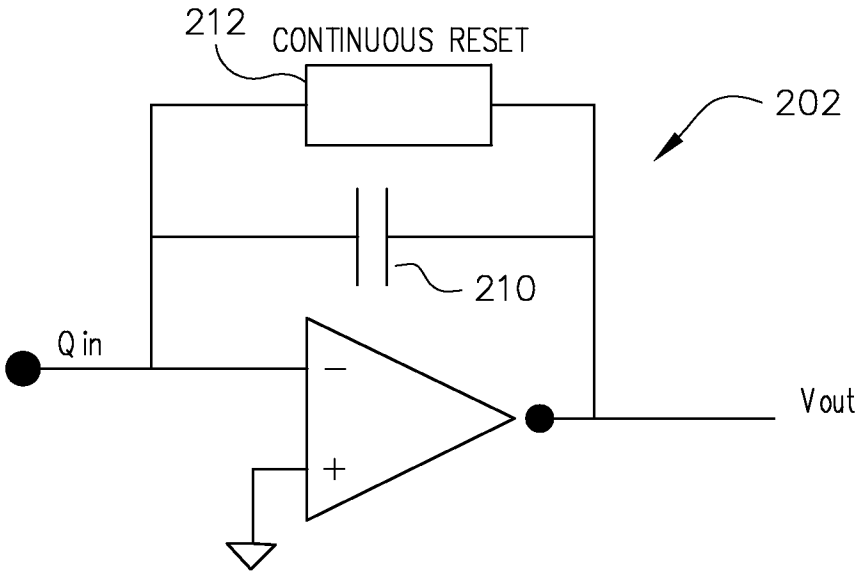

212
CONTINUOUS RESET
202
210
Q in
Vout
−
+

FIG. 10

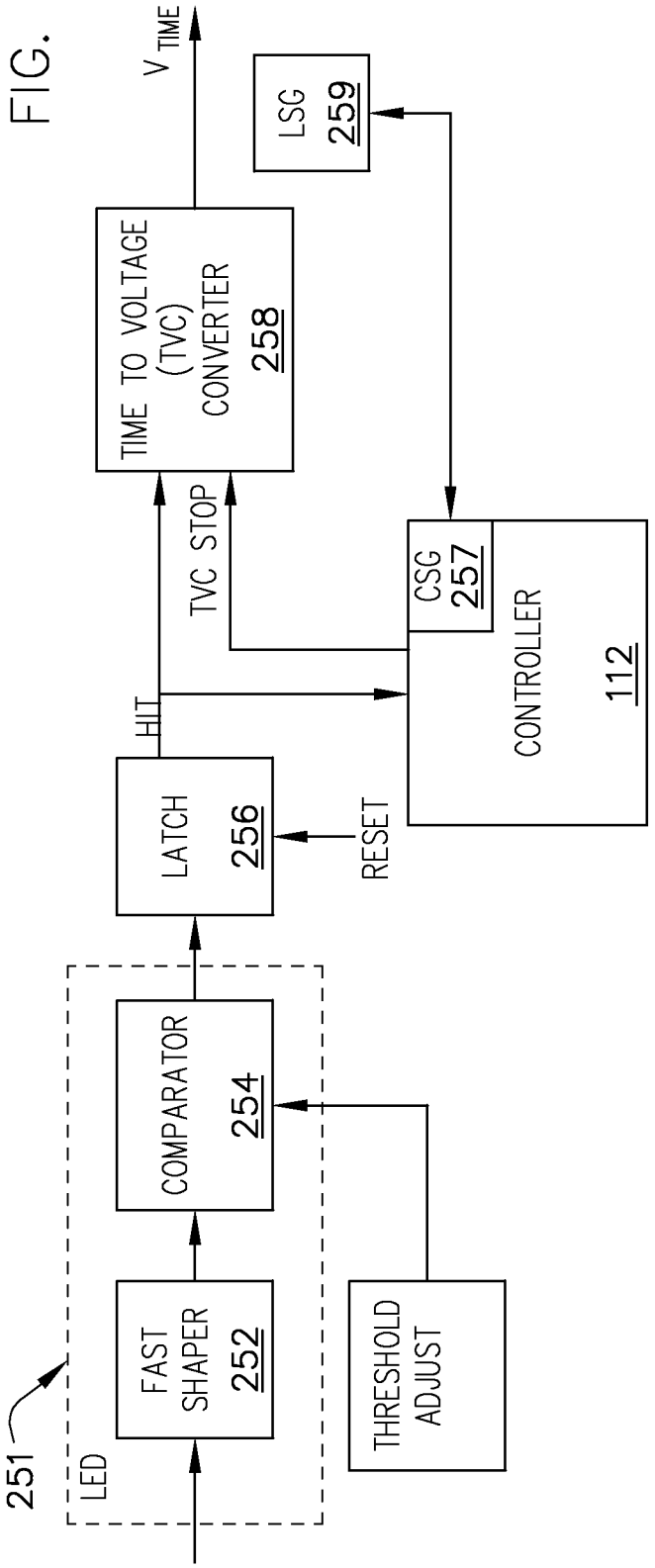


FIG. 11

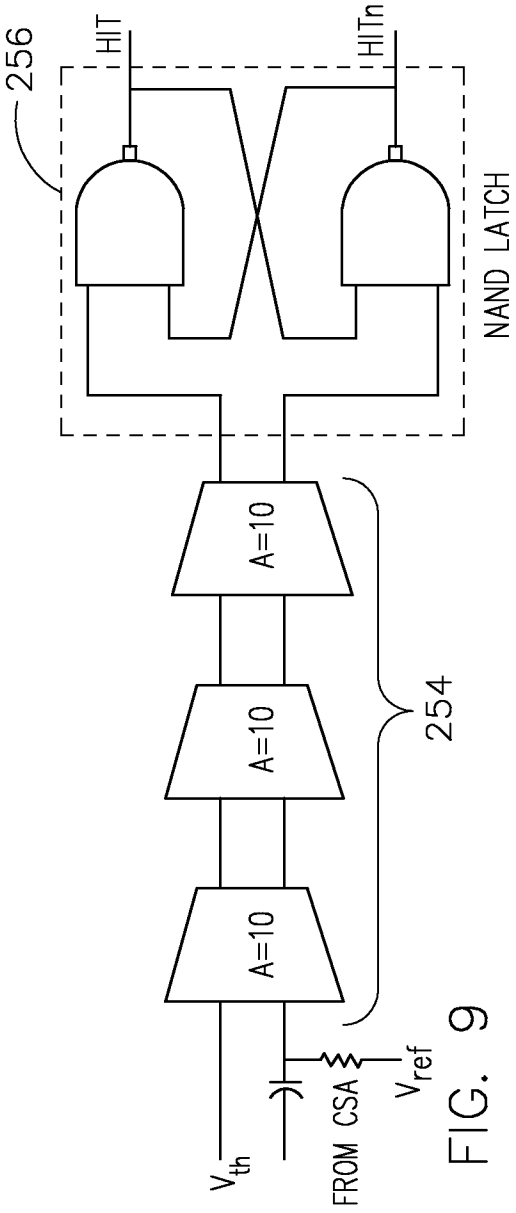
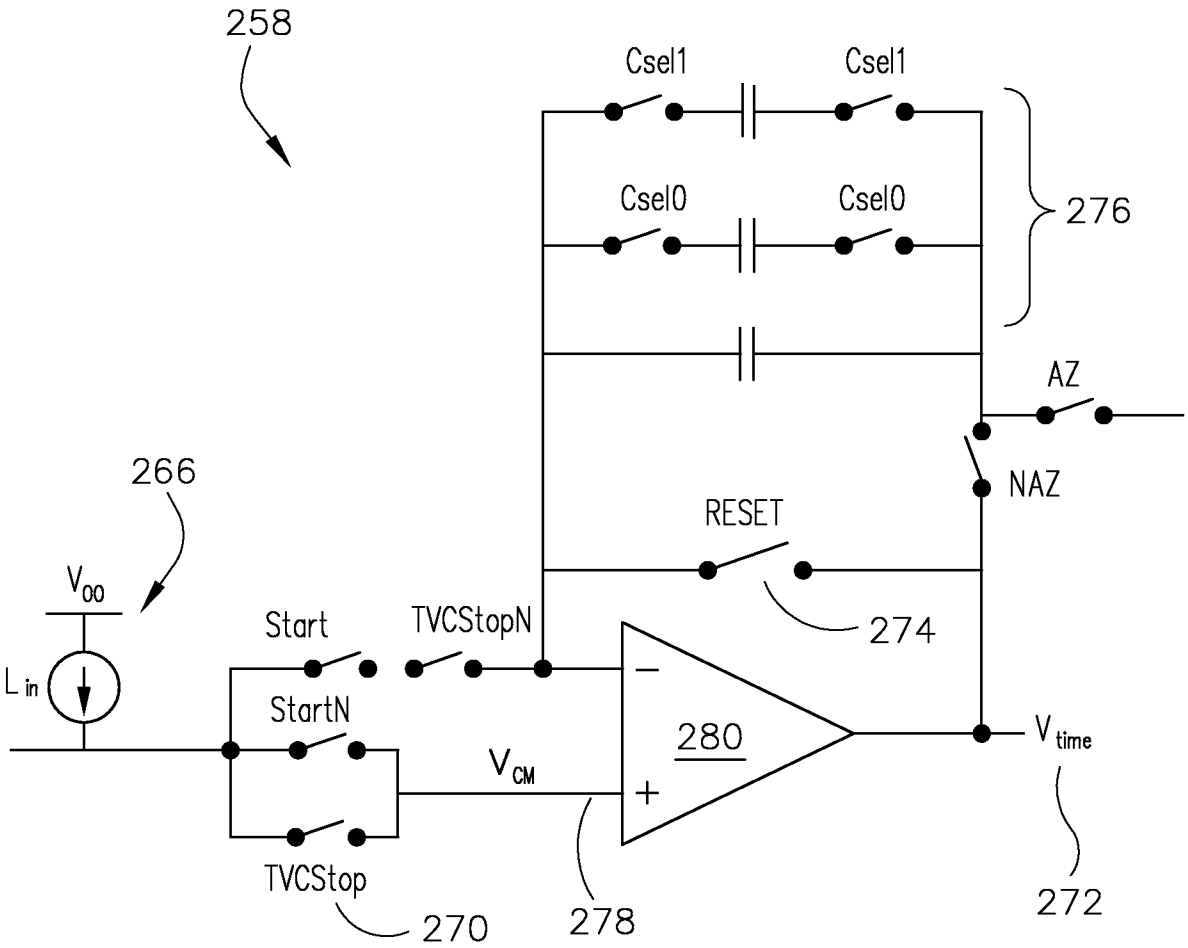


FIG. 9

FIG. 12


258
Csel1
Csel1
Csel0
Csel0
276
AZ
NAZ
266
RESET
V_{00}
Start
TVCStopN
274
L_{in}
StartN
280
V_{time}
V_{CM}
TVCStop
270
278
272

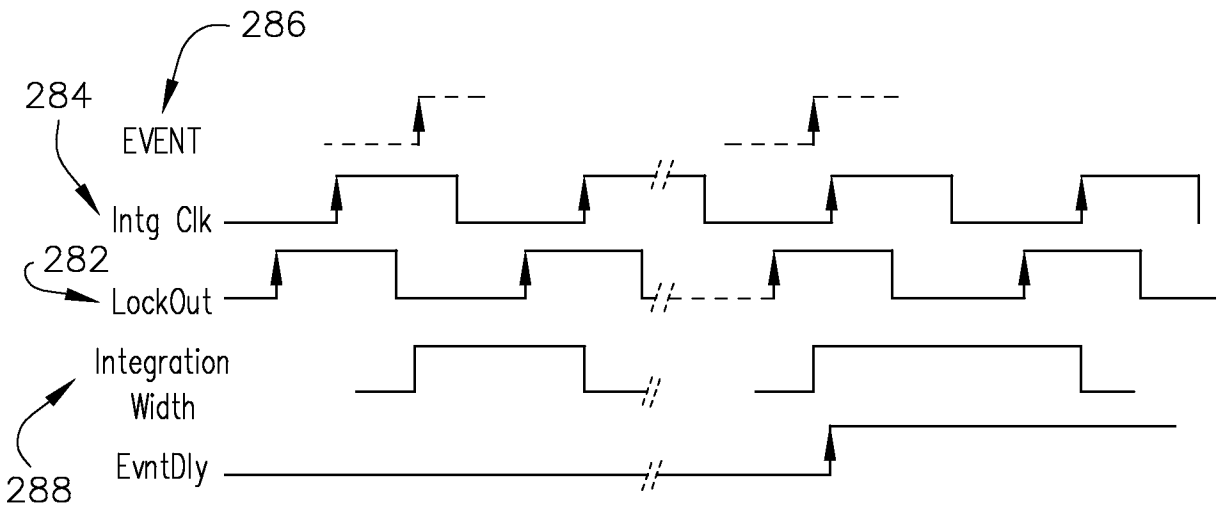

286
284
EVENT
Intg Clk
282
LockOut
Integration
Width
288
EvntDly

FIG. 13

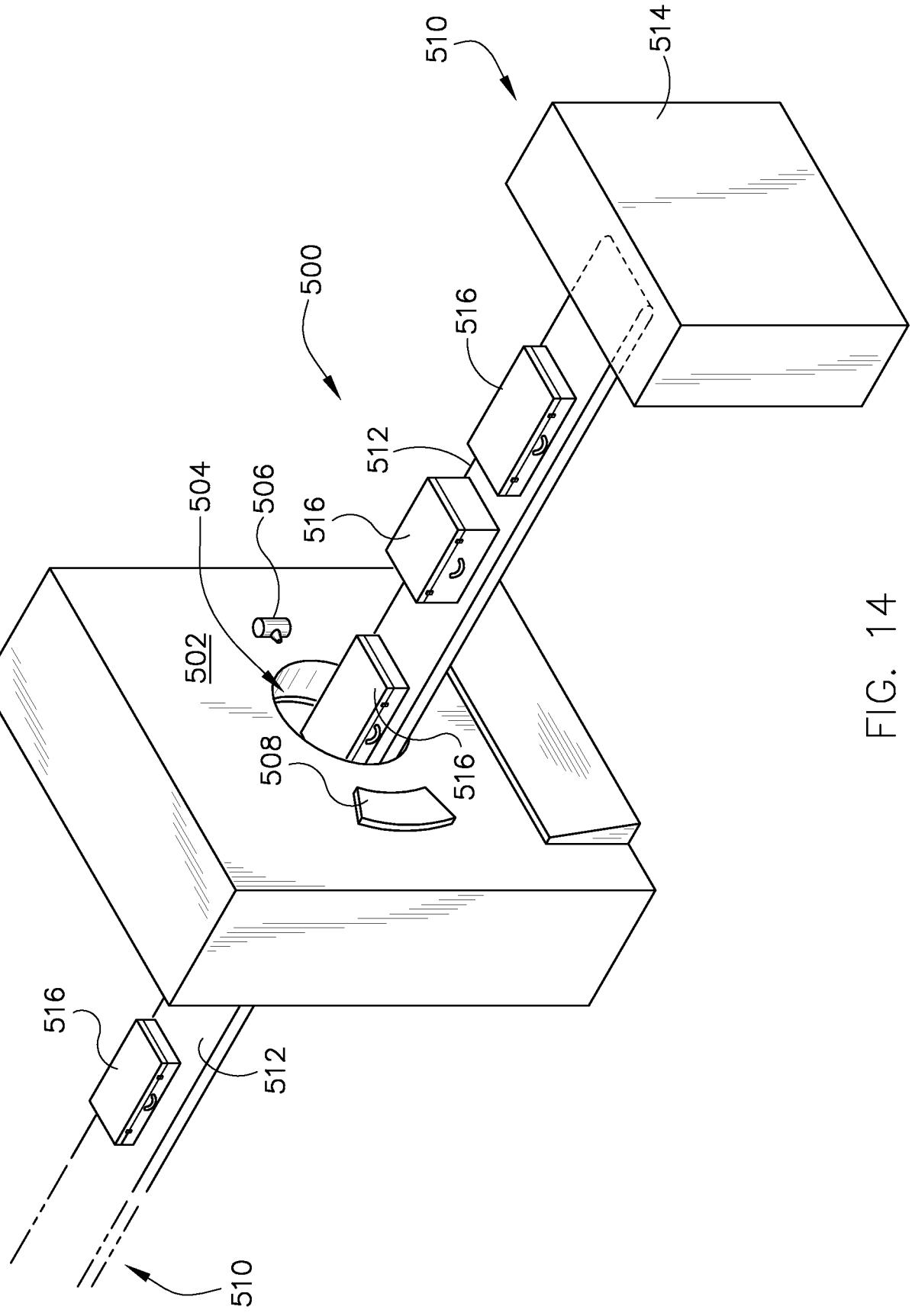


FIG. 14

INTERNATIONAL SEARCH REPORT

International application No
PCT/US2009/048853

A. CLASSIFICATION OF SUBJECT MATTER
INV. G01T1/17

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
G01T

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)
EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 2007/057699 A1 (TUMER TUMAY O [US] ET AL TUEMER TUEMAY O [US] ET AL) 15 March 2007 (2007-03-15) paragraph [0015] paragraph [0018] figure 1 paragraph [0036] paragraphs [0129] - [0131]	1-13
A	US 2007/235657 A1 (HE ZHONG [US] ET AL) 11 October 2007 (2007-10-11) abstract paragraphs [0046], [0047]	1-13

☐ Further documents are listed in the continuation of Box C.

☒ See patent family annex.

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Date of the actual completion of the international search	Date of mailing of the international search report
3 September 2009	11/09/2009

Name and mailing address of the ISA/	Authorized officer
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INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No
PCT/US2009/048853

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2007057699 A1	15-03-2007	NONE	
US 2007235657 A1	11-10-2007	US 2009114829 A1	07-05-2009