



**FOR THE PURPOSES OF INFORMATION ONLY**

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	FR	France	ML	Mali
AU	Australia	GA	Gabon	MR	Mauritania
BB	Barbados	GB	United Kingdom	MW	Malawi
BE	Belgium	HU	Hungary	NL	Netherlands
BG	Bulgaria	IT	Italy	NO	Norway
BJ	Benin	JP	Japan	RO	Romania
BR	Brazil	KP	Democratic People's Republic of Korea	SD	Sudan
CF	Central African Republic	KR	Republic of Korea	SE	Sweden
CG	Congo	LI	Liechtenstein	SN	Senegal
CH	Switzerland	LK	Sri Lanka	SU	Soviet Union
CM	Cameroon	LU	Luxembourg	TD	Chad
DE	Germany, Federal Republic of	MC	Monaco	TG	Togo
DK	Denmark	MG	Madagascar	US	United States of America
FI	Finland				

SPONTANEOUS VESICULATION OF MULTILAMELLAR LIPOSOMES

5

BACKGROUND OF THE INVENTION

10

The present invention is directed to a method of forming unilamellar vesicles without the use of homogenization, filtration, sonication, or extrusion techniques, or other techniques that require energy input to the system, or exposure of lipids to harsh environments. Such environments include for example detergent or extreme pH environments.

15

20

25

Liposomes (vesicles) are completely closed lipid bilayer membranes containing an entrapped aqueous volume. Liposomes may be unilamellar vesicles (possessing a single membrane bilayer) or multilamellar vesicles (onion-like structures characterized by multiple membrane bilayers, each separated from the next by an aqueous layer). The bilayer is composed of two lipid monolayers having a hydrophobic "tail" region and a hydrophilic "head" region. The structure of the membrane bilayer is such that the hydrophobic (nonpolar) "tails" of the lipid monolayers orient towards the center of the bilayer while the hydrophilic "heads" orient towards the aqueous phase.

30

35

The original liposome preparation of Bangham et al. (J. Mol. Biol., 1965, 12:238-252) involves suspending phospholipids in an organic solvent which is then evaporated to dryness leaving a phospholipid film on the reaction vessel. Next, an appropriate amount of aqueous phase is added, the mixture is allowed to "swell," and the resulting liposomes which consist of multilamellar vesicles (MLVs) are dispersed by mechanical means. MLVs so formed may be used in the practice of the present invention.

Another class of multilamellar liposomes that may be used as the starting liposomes of this invention are those characterized as having substantially equal lamellar solute distribution. This class of liposomes is denominated as stable plurilamellar vesicles (SPLV) as defined in U.S. Patent No. 4,522,803 to Lenk, et al., reverse phase evaporation vesicles (REV) as described in U.S. Patent No. 4,235,871 to Papahadjopoulos et al., monophasic vesicles as described in U.S. Patent No. 4,558,579 to Fountain, et al., and frozen and thawed multilamellar vesicles (FATMLV) wherein the vesicles are exposed to at least one freeze and thaw cycle; this procedure is described in Bally et al., PCT Publication No. 87/00043, January 15, 1987, entitled "Multilamellar Liposomes Having Improved Trapping Efficiencies"; these references are incorporated herein by reference.

Liposomes are comprised of lipids; the term lipid as used herein shall mean any suitable material resulting in a bilayer such that a hydrophobic portion of the lipid material orients toward the interior of the bilayer while a hydrophilic portion orients toward the aqueous phase. The lipids which can be used in the liposome formulations of the present invention are the phospholipids such as phosphatidylcholine (PC) and phosphatidylglycerol (PG), more particularly dimyristoylphosphatidylcholine (DMPC) and dimyristoylphosphatidylglycerol (DMPG). Liposomes may be formed and vesiculated using DMPG, or DMPG mixed with DMPC in, for example, a 3:7 mole ratio, respectively.

During preparation of the liposomes, organic solvents may be used to suspend the lipids. Suitable organic solvents are those with intermediate polarities and dielectric properties, which solubilize the lipids, and include but are not limited to halogenated, aliphatic, cycloaliphatic, or aromatic-aliphatic hydrocarbons, such as benzene, chloroform, methylene chloride, or alcohols, such as methanol, ethanol, and solvent mixtures such as benzene:methanol (70:30). As a result, solutions (mixtures in which

the lipids and other components are uniformly distributed throughout) containing the lipids are formed. Solvents are generally chosen on the basis of their biocompatibility, low toxicity, and solubilization abilities.

5

10

15

20

The starting multilamellar liposomes and resulting unilamellar liposomes of the present invention may contain lipid soluble bioactive agents. Such agents are typically associated with the lipid bilayers of the liposomes. As used in the present invention, the term bioactive agent is understood to include any compound having biological activity; e.g., lipid soluble drugs such as non steroidal antiinflammatory drugs such as ibuprofen, indomethacin, sulindac, piroxicam, and naproxen, antineoplastic drugs such as doxorubicin, vincristine, vinblastine, methotrexate and the like, and other therapeutic agents such as anesthetics such as dibucaine, cholinergic agents such as pilocarpine, antihistamines such as benedryl, analgesics such as codeine, anticholinergic agents such as atropine, antidepressants such as imipramine, antiarrhythmic agents such as propranolol, and other lipophilic agents such as dyes, therapeutic proteins and peptides such as immunomodulators, radio-opaque agents, fluorescent agents, and the like. Additionally, the vesicles made by the process of this invention may contain bilayer-associated markers or molecules such as proteins or peptides.

25

30

The liposomes of the invention may be used in a liposome-drug delivery system. In a liposome-drug delivery system, a bioactive agent such as a drug is associated with the liposomes and then administered to the patient to be treated. For example, see Rahman et al., U.S. Patent No. 3,993,754; Sears, U.S. Patent No. 4,145,410; Papahadjopoulos et al., U.S. Patent No. 4,235,871; Schnieder, U.S. Patent No. 4,224,179; Lenk et al., U.S. Patent No. 4,522,803; and Fountain et al., U.S. Patent No. 4,588,578.

35

Many drugs that are useful for treating disease show toxicities in the patient; such toxicities may be cardiotoxicity, as with the

antitumor drug doxorubicin, or nephrotoxicity, as with the aminoglycoside or polyene antibiotics such as amphotericin B. Amphotericin B is an extremely toxic antifungal polyene antibiotic with the single most reliability in the treatment of life-threatening fungal infections (Taylor et al., Am. Rev. Respir. Dis., 1982, 125:610-611). Because amphotericin B is a hydrophobic drug, it is insoluble in aqueous solution and is commercially available as a colloidal dispersion in desoxycholate, a detergent used to suspend it which in itself is toxic. Amphotericin B methyl ester and amphotericin B have also been shown to be active against the HTLV-III/LAV virus, a lipid-enveloped retrovirus, shown in the etiology of acquired immuno-deficiency syndrome (AIDS) (Schaffner et al., Biochem. Pharmacol., 1986, 35:4110-4113). In this study, amphotericin B methyl ester ascorbic acid salt (water soluble) and amphotericin B were added to separate cultures of HTLV-III/LAV infected cells and the cells assayed for replication of the virus. Results showed that amphotericin B methyl ester and amphotericin B protected target cells against the cytopathic effects of the virus, similar to that demonstrated for the herpes virus (Stevens et al., Arch. Virol., 1975, 48:391).

Reports of the use of liposome-encapsulated amphotericin B have appeared in the literature. Juliano et al. (Annals N. Y. Acad. Sci., 1985, 446:390-402) discuss the treatment of systemic fungal infections with liposomal amphotericin B. Such liposomes comprise phospholipid, for example dimyristoylphosphatidylcholine (DMPC) and dimyristoylphosphatidylglycerol (DMPG) in a 7:3 mole ratio, and cholesterol. Acute toxicity studies ( $LD_{50}$ s) and *in vitro* assays comparing free and liposome-entrapped amphotericin B showed lower toxicities using the liposomal preparations with substantially unchanged antifungal potency. Lopez-Berestein et al. (J. Infect. Dis., 1986, 151:704-710) administered liposome-encapsulated amphotericin B to patients with systemic fungal infections. The liposomes comprised a 7:3 mole ratio of DMPC:DMPG, and the drug was encapsulated at a greater than 90% efficiency. As a result of the liposomal-drug treatment at 5 mol % amphotericin B, 66% of the

patients treated responded favorably, with either partial or complete remission of the fungal infection. Lopez-Berestein et al. (J. Infect. Dis., 1983, 147:939-945), Ahrens et al., (S. Jour. Med. Vet. Mycol., 1984, 22:161-166), Panosian et al. (Antimicrob. Agents Chemo., 1984, 25:655-656), and Tremblay et al. (Antimicrob. Agents Chemo., 1984, 26:170-173) also tested the comparative efficacy of free versus liposomal amphotericin B in the treatment and prophylaxis of systemic candidiasis and leishmaniasis (Panosian et al., supra.) in mice. They found an increased therapeutic index with the liposome-encapsulated amphotericin B in the treatment of candidiasis. In all cases, it was found that much higher dosages of amphotericin B may be tolerated when this drug is encapsulated in liposomes. The amphotericin B-liposome formulations had little to no effect in the treatment of leishmaniasis.

The ability of liposomes to buffer the toxicity of entrapped drugs with little or no decrease in efficacy is becoming increasingly well established. Therefore, there is an increasing need to be able to form liposomes of all types which have these qualities. Unilamellar vesicles are clearly preferred for certain types of in vivo drug delivery over multilamellar vesicles, as well as for studies of membrane-mediated processes. As used as in vivo delivery vehicles, for example, unilamellar vesicles are cleared more slowly from the blood than are MLVs, and exhibit an enhanced distribution to the lungs and possibly bone marrow. Up to the time of the present invention, the methods known for producing these type vesicles relied upon harsh treatment of multilamellar vesicles, such as extrusion through filters, or other physically damaging processes requiring energy input such as sonication, homogenization or milling. Chemical treatment techniques employing harsh detergents or solutions at high or low pH to form unilamellar vesicles have also been employed. The present invention advances the art in that it allows formation of unilamellar vesicles from multilamellar vesicles without the heretofore harsh treatments required, but through the incubation of the liposomes in low ionic strength media at selected temperatures.

5 Additionally, the unexpected simplicity of preparation of these systems is complemented by the highly defined conditions under which they may be formed. The fact that vesiculation of these lipids occurs only around about the lipid phase transition temperature ( $T_c$ ) and under low ionic strength incubations gives one a high degree of control over vesicle formation. In addition, the characteristic bilayer instability of these systems would be expected to favor interaction of the bilayer with hydrophobic compounds such as drugs, or enhance insertion of membrane proteins or peptides.

10

#### SUMMARY OF THE INVENTION

15 The present invention discloses a method for spontaneously forming unilamellar vesicles from multilamellar vesicles (MLVs). Such MLVs comprise lipids, and unilamellar vesicles are formed by incubating the multilamellar vesicles in low ionic strength medium at neutral pH, around about the transition temperature of the lipids. Preferably the lipids comprise phospholipids, specifically  
20 phosphatidylglycerol alone or in combination with phosphatidylcholine, more specifically dimyristoylphosphatidylcholine and dimyristoylphosphatidylglycerol, in a 7:3 mole ratio.

25

To form the unilamellar vesicles of the invention, the liposomes are incubated at about 22-26°C, preferably about 24°C in a medium of between about 0 mM and 25 mM salt. More preferably, the medium  
30 comprises about 0 - 10mM salt at pH of about 7.0 to about 8.0, preferably pH 7.6 and incubation time is about 15 minutes to about 24 hours.

35



BRIEF DESCRIPTION OF THE DRAWING

FIGURE 1 demonstrates vesiculation of DMPC:DMPG (7:3) MLVs as a function of ionic strength of the incubation medium. DMPC:DMPG (10mM) was hydrated at 4°C in the media shown below and incubated at 24°C (see Examples 1 and 2). Sample media were H<sub>2</sub>O (open circles); 2mM HEPES (closed squares); 10mM NaCl, 2mM HEPES, pH 7.6, (open triangles); or 25 mM NaCl, 2 mM HEPES, pH 7.6 (closed triangles).

FIGURE 2 are <sup>31</sup>P-NMR spectra of DMPC:DMPG. Lipid (10 mM) was hydrated in H<sub>2</sub>O at 4°C and its spectrum was recorded at 30°C (A). The same lipid mixture was then incubated at 24°C for 1 hour (B) and 12 hours (C). DMPC:DMPG (7:3 mole ratio) hydrated in 150 mM NaCl, 10 mM HEPES, pH 7.6 and incubated at 24°C for 12 hours is shown in (D).

FIGURE 3 are <sup>31</sup>P-NMR spectra for mixtures of phosphatidylcholine with phosphatidylglycerol. Lipid (10 mM) was hydrated in 150 mM NaCl, 10 mM HEPES, pH 7.6 (A,B,C,) or 2 mM HEPES, pH 7.6 (D,E,F,G,H,J) and incubated at 24°C (A,B,C,G,H,J) or 10°C (D,E,F) for 16 hours.

DETAILED DESCRIPTION OF THE INVENTION

The unilamellar liposomes of this invention are formed by the exposure of multilamellar liposomes to conditions of low ionic strength media at neutral pH, and incubation temperatures around about the gel-to-liquid crystalline transition temperature (T<sub>c</sub>). Under such incubation conditions, MLVs vesiculate to form unilamellar vesicles. Prior art techniques requiring acidic and alkaline pH variations are not needed in the present method, as vesiculation takes place in a narrow range around neutral pH. The

liposomes of the present invention are preferably comprised of phospholipids, specifically dimyristoylphosphatidylglycerol (DMPG) or with dimyristoylphosphatidylcholine (DMPC). Various mole ratios of DMPC and DMPG are suitable for liposome vesiculation, however, the rate of vesiculation decreases with decreasing DMPG concentration.

Upon hydration most naturally occurring phospholipids generally adopt either the bilayer organization or the hexagonal  $H_{II}$  phase (Gullis and de Kruijff, 1979, *Biochim. Biophys. Acta*, 559:339; Gullis et al., 1985, *in Phospholipids and Cellular Regulation*, J. F. Kuo, Ed., CRC Press, Boca Raton, Florida). In both instances the macromolecular structures formed are large (several microns) and are stable, such that even transitions between these two polymorphic phases do not generate small vesicles. One exception is the case of cardiolipin which in the presence of calcium adopts the hexagonal  $H_{II}$  phase. If this mixture is dialyzed against EDTA, small vesicles are generated (Vail et al., 1979, *Biochim. Biophys. Acta*, 551:74). However, this is presumably due to the removal of calcium from cardiolipin at the exterior of the cylindrical  $H_{II}$  arrays and the consequent "blebbing-off" of bilayer vesicles. While large multilamellar vesicles are useful membrane models for investigating the structural and motional properties of lipids, many areas of membrane research and drug delivery require or favor, respectively, the use of unilamellar vesicle systems. Two categories of unilamellar vesicles can be defined. These are small unilamellar vesicles (SUVs) of diameter less than about 50 nm, and large unilamellar vesicles (LUVs) which generally encompass vesicles 50 nm to 1 micron in diameter (Hope et al., 1986, *Chem. Phys. Lip.*, 40:89).

The absence of multiple internal aqueous compartments and the relatively high trapped volumes obtained with LUVs make them useful in a variety of research areas including membrane fusion (Wilschut et al., 1980, *Biochemistry*, 19:6011) and the *in vivo* delivery of biologically active compounds (Poznansky et al., 1984, *Pharmacol. Rev.*, 36:227). While MLVs formed by the simple hydration of dry

lipid are under osmotic stress due to non-equilibrium solute distribution (Gruner et al., 1985, *Biochemistry*, 24:2833; Mayer et al., 1986, *Biochim. Biophys. Acta*, 858:161), they are nevertheless stable structures. The formation of LUVs or SUVs from MLVs usually requires aggressive disruption, for example, by sonication (Huang, 5 1969, *Biochemistry*, 8:344) or extrusion through polycarbonate filters (Hope et al., 1985, *Biochim. Biophys. Acta*, 812, 55), as mentioned above.

While the formation of LUVs from mixtures of phosphatidylcholine with either charged single chain detergents (Hauser et al., 1986, 10 *Biochemistry*, 25:2126) or short chain phospholipids (Gabriel et al., 1984, *Biochemistry*, 23:4011) has been described, the only reported instance of MLVs composed solely of bilayer-forming phospholipids spontaneously vesiculating concerns mixtures of acidic phospholipids 15 and phosphatidylcholine transiently exposed to an alkaline pH (Hauser et al., 1982, *Proc. Natl. Acad. Sci USA*, 79:1683; Hauser, U.S. Patent No. 4,619,794, issued October 28, 1986, Hauser et al., 1986, *Biochemistry*, 25:2126; Gains et al., 1983, *Biochim. Biophys. Acta*, 731:31; Li et al., 1986, *Biochemistry*, 25:7477).

Since the exposure of membrane lipids to alkaline pH may result in degradation of the lipids and/or any bioactive agent present, and leakage of the vesicle contents, this technique has severe 20 shortcomings in the field of drug delivery employing liposomes. We disclose here that formation of unilamellar vesicles can surprisingly occur at around neutral pH for saturated 25 phosphatidylglycerol and mixtures of saturated phosphatidylcholine and phosphatidylglycerol. Unexpectedly, vesiculation is rapid only at temperatures around the gel to liquid-crystalline phase 30 transition (the transition temperature or  $T_c$ , about 22°C to about 26°C, most preferably about 24°C), and when hydration or incubation media of low ionic strength are used. When incubation media of high ionic strength (higher than about 50 mM salt) are used, vesiculation occurs at a decreased rate, or not at all. Vesiculation occurs as a 35 function of lowering the ionic strength of the incubation medium.

MLVs vesiculate spontaneously when exposed to low ionic strength incubation media (about 10 mM ionic strength and less) when incubated around about the  $T_c$  of the lipid. Any ionic species solutions may be used as incubation media, such as the salts sodium chloride, potassium chloride, and others. While a range, therefore, of about 0-25 mM salt in the incubation medium will promote vesiculation, the optimum conditions are around about 0-10 mM salt.

Vesiculation of MLV systems may be determined by incubating the liposomes in low ionic strength medium for 15 minutes to several hours, at around the gel-to-liquid crystalline transition temperature of the lipids used. Whether vesiculation has occurred may be measured by the size of the resulting liposomes using quasi-elastic light scattering, (unilamellar versus multilamellar), visualization of the resulting vesicles using freeze-fracture electron microscopy, and  $^{31}\text{P}$ -NMR analysis of lineshape and spectrum width. For example, narrow spectrum width and isotropic signal is indicative of unilamellar vesicle structure, while a low field shoulder and high field peaks are indicative of larger vesicles.

Liposomes incorporating a bioactive agent, such as a drug, such as for example, amphotericin B may be formed according to the processes of the invention as follows. Amphotericin B is suspended in an aqueous solution, for example distilled water, by sonication. The suspended drug is then admixed with a suspension of lipid in aqueous solution, such as distilled water or sodium chloride solution. The mixture is incubated at or above the transition temperature of the lipid employed, with the resultant formation of vesicles.

Where dimyristoylphosphatidylglycerol (DMPG) is used alone or in combination to form the liposomes, and when the lipid has been admixed with an aqueous solution having an ionic strength of about 0 mM to about 25 mM salt, and incubated at about the transition temperature ( $T_c$ ) of the lipid (i.e., at about 22-24°C), the

liposomes spontaneously vesiculate, forming large unilamellar vesicles (LUVs). This method for formation of LUVs, which employs no harsh treatment of the vesicles such as exposure to chemicals, detergents, or extreme pH, is disclosed in copending U.S. Patent Application Serial No. 136,267, filed December 22, 1987, relevant portions of which are incorporated herein by reference.

For example, DMPG can be used alone or, for example, with other lipid such as with DMPC, e.g., in a 3:7 mole ratio of DMPC:DMPG. These lipids can be co-lyophilized from a 70:30 v/v solution of benzene:methanol, and stored at  $-20^{\circ}\text{C}$  until use. MLVs are prepared by hydrating the lipid (for example, a total of lipid of 13.5 umoles/ml) in aqueous solution such as distilled water or buffer at  $4^{\circ}\text{C}$ . When formation of amphotericin B-containing LUVs is desired, the lipid is hydrated in an aqueous solution of ionic strength of about ) mM to about 25 mM salt, and incubated at aout  $23^{\circ}\text{C}$ . Amphotericin B, dispersed in distilled water by bath sonication, at a concentration of about 0.98 umoles/ml is then added to the hydrated lipid and incubated at about  $23^{\circ}\text{C}$  for about one hour, resulting in LUVs containing amphotericin B. These proportions of lipid and amphotericin B result in about a 7 mole % ratio of amphotericin B.

The lipids of the present invention may be hydrated to form liposomes using any available aqueous solutions, for example, distilled water, saline, or aqueous buffers. Such buffers include but are not limited to buffered salines such as phosphate buffered saline ("PBS"), tris-(hydroxymethyl)-aminomethane hydrochloride ("tris") buffers, and preferably N-2-hydroxyethyl piperazine-N-2-ethane sulfonic acid ("HEPES") buffer. Such buffers are preferably used at pH of about 7.0 to about 8.0, preferably about pH 7.6. If required, the ionic strength of the medium may be adjusted to physiological values following the vesiculation procedure.

5 The liposomes of the present invention may be dehydrated either prior to or following vesiculation, thereby enabling storage for extended periods of time until use. Standard freeze-drying equipment or equivalent apparatus may be used to lyophilize the liposomes. Liposomes may also be dehydrated simply by placing them under reduced pressure and allowing the suspending solution to evaporate. Alternatively, the liposomes and their surrounding medium may be frozen prior to dehydration. Such dehydration may be performed in the presence of one or more protectants such as protective sugars, according to the process of Janoff et al., PCT 10 86/01103, published February 27, 1986, and incorporated herein by reference.

15 The liposomes resulting from the processes of the present invention can be used therapeutically in mammals, including man, in the treatment of infections or conditions which benefit from the employment of liposomes which give for example, sustained release, reduced toxicity, and other qualities which deliver the drug in its bioactive form.

20 The mode of administration of the preparation may determine the sites and cells in the organism to which the compound will be delivered. The liposomes of the present invention can be administered alone but will generally be administered in admixture with a pharmaceutical carrier selected with regard to the intended route of administration and standard pharmaceutical practice. The 25 preparations may be injected parenterally, for example, intra-arterially or intravenously. The preparations may also be administered via oral, subcutaneous, or intramuscular routes. For parenteral administration, they can be used, for example, in the form of a sterile aqueous solution which may contain other solutes, for example, enough salts or glucose to make the solution isotonic. 30 Other uses, depending upon the particular properties of the preparation, may be envisioned by those skilled in the art.

35

For the topical mode of administration, the liposomes of the present invention may be incorporated into dosage forms such as gels, oils, emulsions, and the like. Such preparations may be administered by direct application as a cream, paste, ointment, gel, lotion or the like.

5

For the oral mode of administration, the liposomes of this invention encapsulating a bioactive agent can be used in the form of tablets, capsules, lozenges, troches, powders, syrups, elixirs, aqueous solutions and suspensions, and the like. In the case of tablets, carriers which can be used include lactose, sodium citrate and salts of phosphoric acid. Various disintegrants such as starch, and lubricating agents, such as magnesium stearate, sodium lauryl sulfate and talc, are commonly used in tablets. For oral administration in capsule form, useful diluents are lactose and high molecular weight polyethylene glycols. When aqueous suspensions are required for oral use, the active ingredient is combined with emulsifying and suspending agents. If desired, certain sweetening and/or flavoring agents can be added.

10

15

20

The following examples are given for purposes of illustration only and not by way of limitation on the scope of the invention.

#### EXAMPLE 1

25

DMPC:DMPG (7:3 M ratio) was lyophilized from benzene:methanol (70:30 v/v). The lipid was hydrated to 10 mM with distilled water pH 7.6, at 4°C, forming MLVs. The suspension was then incubated at 24°C for 15 minutes. QELS studies showed the resulting liposomes to be about 200 nm in diameter, corresponding to LUVs.

30

The above procedure was followed using 2 mM HEPES buffer as the hydrating solution. QELS measurements revealed LUVs.

35

This Example demonstrates the formation of unilamellar liposomes by the incubation of a 7:3 M ratio of DMPC:DMPG in low ionic strength medium (distilled water, 0 mM salt), at neutral pH. Unilamellar liposomes formed spontaneously when the preparation was incubated at 24°C.

5

#### EXAMPLE 2

The procedures and materials of Example 1 were employed using 150 mM NaCl, 2 mM HEPES buffer as the hydrating solution. QELS measurements revealed no change in liposome size (no vesiculation) after incubation.

10

Figure 1 demonstrates vesiculation by plotting the vesicle diameter (obtained by quasi elastic light scattering, QELS) as an indication of MLV or LUV against time of incubation, and shows that the rate of vesiculation at 24°C is directly related to the ionic strength of the hydration medium. Figure 2 demonstrates the vesiculation by <sup>31</sup>P-NMR spectra of the suspensions; the vesiculated samples (B and C, at low ionic strength incubation) demonstrate the characteristic narrow spectrum and isotropic lipid motion peak which would be expected for vesicles smaller than 400 nm. Figure 2 A and D demonstrate the characteristic bilayer lineshape with low field shoulder and two high field peaks. Plots A and D were recorded from samples incubated under conditions where vesiculation does not occur; at temperatures above the T<sub>c</sub>, and hydration media of high ionic strength, respectively.

15

20

25

Freeze fracture electron microscopy confirmed the QELS and <sup>31</sup>P-NMR data by allowing visualization of the multilamellar or unilamellar vesicles.

30

35



EXAMPLE 3

5 DMPG (10 mM) was hydrated with 10 mM NaCl, 2 mM HEPES at 4°C, pH 7.6, forming MLVs. These MLVs were incubated at 24°C for 15 minutes, and the sample analyzed by QELS. The resulting liposomes were unilamellar (LUVs).

10 This Example may be compared with Example 13, where liposomes made of a 3:7 M ratio of DMPC:DMPG incubated in 10mM NaCl (Example 13) only approach the 200 nm diameter vesicles of Example 3 after 5 hours incubation.

EXAMPLE 4

15 A 7:3 M ratio of dry DMPC:DMPG was equilibrated at 32°C in a water-saturated atmosphere for 60 minutes, and then the procedures and materials of Example 1 were followed to make MLVs (10 mM lipid), using 2 mM HEPES as hydration medium and an incubation temperature of 32°C. After 6 hours incubation, no vesiculation had occurred as QELS measurements revealed the liposomes had a mean diameter of 20 greater than 2 microns.

25 The above preparation was then incubated at 24°C and QELS measurements revealed that the liposomes had vesiculated, resulting in unilamellar vesicles.

30 This Example is a control for the incubation of the liposome systems around about the  $T_c$  of the lipid; it shows this incubation parameter is an important requirement of the invention.

EXAMPLE 5

35 The procedures and materials of Example 4 were employed using 2 mM HEPES as the hydration medium and an incubation temperature of 15°C. After 6 hours incubation, no vesiculation had occurred as

QELS measurements revealed the liposomes had a mean diameter greater than 2 microns.

5 The above preparation was then incubated at 24°C and QELS measurements revealed that the liposomes had vesiculated, resulting in unilamellar vesicles.

10 This Example serves as a further control for  $T_c$  being an important incubation parameter. No vesiculation occurred at this incubation temperature. However, when this system was incubated at 24°C, the liposomes rapidly vesiculated.

#### EXAMPLE 6

15 A 7:3 M ratio of DOPC:DOPG was hydrated with 2 mM HEPES buffer and incubated for 24 hours at 24°C. Samples were analyzed using  $^{31}\text{P}$ -NMR spectroscopy which had a spectrum consistent with bilayer phase lipid organization (Figure 6K), and the vesicles had a diameter greater than about 400 nm.

#### EXAMPLE 7

25 The procedures and materials of Example 1 were employed, using a 7:3 M ratio of DOPC:DMPC. The lipid was hydrated with 2 mM HEPES and incubated at 24°C for 16 hours.

$^{31}\text{P}$ -NMR spectroscopy revealed little or no vesiculation.

#### EXAMPLE 8

35 The procedures and materials of Example 7 were employed, using a 7:3 M ratio of DMPC:DOPG. The lipid was hydrated with 2 mM HEPES and incubated at 24°C for 16 hours.

<sup>31</sup>P-NMR spectroscopy revealed little or no vesiculation.

#### EXAMPLE 9

5

The procedures and materials of Example 7 were employed, using a 7:7:3:3 M ratio of DOPC:DMPC:DOPG:DMPG. The lipid was hydrated with 2 mM HEPES and incubated at 24°C for 16 hours.

10

<sup>31</sup>P-NMR spectroscopy revealed little or no vesiculation.

15

In this Example, when the gel and liquid-crystalline domains contain both phospholipid species, e.g., DMPC:DOPG:DMPG:DOPG (7:7:3:3), only very limited breakdown of MLV structure is apparent. In these systems the presence of dioleoyl phospholipids stabilizes MLV structure. This Example demonstrates the stability of oleoyl-containing systems. Even when phosphatidylglycerol is present, the dioleoyl species stabilizes mixtures of 7:3 M ratio DOPC:DOPG so that incubation at 24°C in low ionic strength buffer does not induce vesiculation; the systems remain multilamellar.

20

25

Further, the stabilizing nature of dioleoyl chains is observed in Examples 7-12 where no vesiculation is observed even when domains of both gel phase lipid (i.e.: dimyristoyl chains) and liquid crystalline phase lipid (i.e.: dioleoyl groups) are present. Figure 3 (A-J) demonstrates the <sup>31</sup>P-NMR spectra for such samples incubated at either 10°C or 24°C. All spectra are characteristic of large vesicles in the bilayer phase (MLVs); the samples did not vesiculate.

30

#### EXAMPLE 10

35

The procedures and materials of Example 7 were employed, using a 7:3 M ratio of DOPC:DMPG. The lipid was hydrated with 150 mM NaCl,

2 mM HEPES and incubated for 16 hours at 24°C.

<sup>31</sup>P-NMR spectroscopy revealed little or no vesiculation.

5

EXAMPLE 11

The procedures and materials of Example 7 were employed, using a 7:3 M ratio of DMPC:DOPG. The lipid was hydrated with 150 mM NaCl, 2 mM HEPES and incubated for 16 hours at 24°C.

10

<sup>31</sup>P-NMR spectroscopy revealed little or no vesiculation.

15

EXAMPLE 12

The procedures and materials of Example 7 were employed, using a 7:7:3:3 M ratio of DOPC:DMPC:DOPG:DMPG. The lipid was hydrated with 150 mM NaCl, 2 mM HEPES and incubated for 16 hours at 24°C.

20

<sup>31</sup>P-NMR spectroscopy revealed little or no vesiculation.

EXAMPLE 13

25

The procedures and materials of Example 3 were employed, using a 3:7 M ratio of DMPC:DMPG. The lipid was hydrated in 10 mM NaCl, 2 mM HEPES at pH 7.6 at 4°C, forming MLVs. The suspension was then incubated for 1 hour at 24°C. QELS measurements revealed that vesiculation of the MLVs had formed LUVs.

30

EXAMPLE 14

Lipid (14.8 umol/ml, 7:3 mol ratio of DMPC:DMPG) was hydrated in distilled water and incubated at 4°C. The resulting MLVs were extruded through two stacked polycarbonate filters ten times using

35

the LUVET procedure.

Amphotericin B was dispersed in distilled water using a bath sonicator at a concentration of 10.8  $\mu\text{mol/ml}$ . The amphotericin B dispersion was added to the lipid suspension to a final lipid and amphotericin B concentration of 13.5  $\mu\text{mol/ml}$  and 0.98  $\mu\text{mol/ml}$ , respectively. To remove unincorporated amphotericin B, 20 ml of the sample were centrifuged at 15,000 X g for 30 minutes in a Ti60 or SW 27 rotor (Beckman) at 22°C in a Beckman L8-60 ultracentrifuge. The supernatant free amphotericin B was removed without disturbing the liposome pellet. The resulting liposomes were measured by quasi-elastic light scattering to be larger than 1.0  $\mu\text{m}$  in diameter.

The above procedure employing incubation conditions of 23°C were repeated employing 150 mM NaCl, 10 mM  $\text{Na}_2\text{PO}_4$ , pH 7.4 to hydrate the lipids. The resulting liposomes were measured by quasielastic light scattering to be larger than 1.0  $\mu\text{m}$  in diameter. Rate of amphotericin B uptake by liposomes was highest when the ionic strength of the medium was low (distilled water vs. 150 mM NaCl).

#### EXAMPLE 15

The materials and procedures of Example 14 were employed, but wherein the lipid suspended in distilled water was incubated with the amphotericin B at 22°C. The resulting liposomes were unilamellar and measured at about 0.1 - 0.2  $\mu\text{m}$  in mean diameter by quasi elastic light scattering.

What is claimed is:

- 5 1. A method for spontaneously forming unilamellar vesicles from multilamellar vesicles comprising dimyristoylphosphatidylglycerol by incubating the multilamellar vesicles in low ionic strength medium at neutral pH, at about  
10 the gel-to-liquid crystalline transition temperature of the lipid.
2. The method of claim 1 wherein the multilamellar vesicles additionally comprise dimyristoylphosphatidylcholine.
- 15 3. The method of claim 2 wherein the dimyristoylphosphatidylcholine and dimyristoylphosphatidylglycerol are in a 7:3 mole ratio.
4. The method of claim 3 wherein the liposomes are incubated at  
20 about 24°C.
5. The method of claim 2 wherein the liposomes are incubated in medium of between about 0 mM and 25 mM salt.
- 25 6. The method of claim 5 wherein the liposomes are incubated in medium of about 10 mM salt for about 15 minutes.
7. The method of claim 1 wherein the liposomes are incubated in medium at pH of about 7.0 to about 8.0.
- 30 8. The method of claim 7 wherein the liposomes are incubated in medium at about pH 7.6.
- 35 9. A method for spontaneously forming unilamellar vesicles from multilamellar vesicles comprising dimyristoylphosphatidylglycerol by incubating the multilamellar vesicles in medium of about 10 mM salt for about 15 minutes at about 24°C at pH about 7.6.

10. The method of claim 9 wherein the liposomes additionally comprise dimyristoylphosphatidylcholine.

5 11. A method for preparing a composition comprising a liposome comprising a drug and a lipid in a high drug:mol ratio, wherein the method comprises the steps of:

(a) suspending a drug in an aqueous solution;

10 (b) suspending a lipid in an aqueous solution;

(c) admixing the products of steps (a) and (b); and

15 (d) incubating the product of step (c) at or above the transition temperature of the lipid.

12. The method of claim 11 wherein the drug is suspended in aqueous solution by sonication.

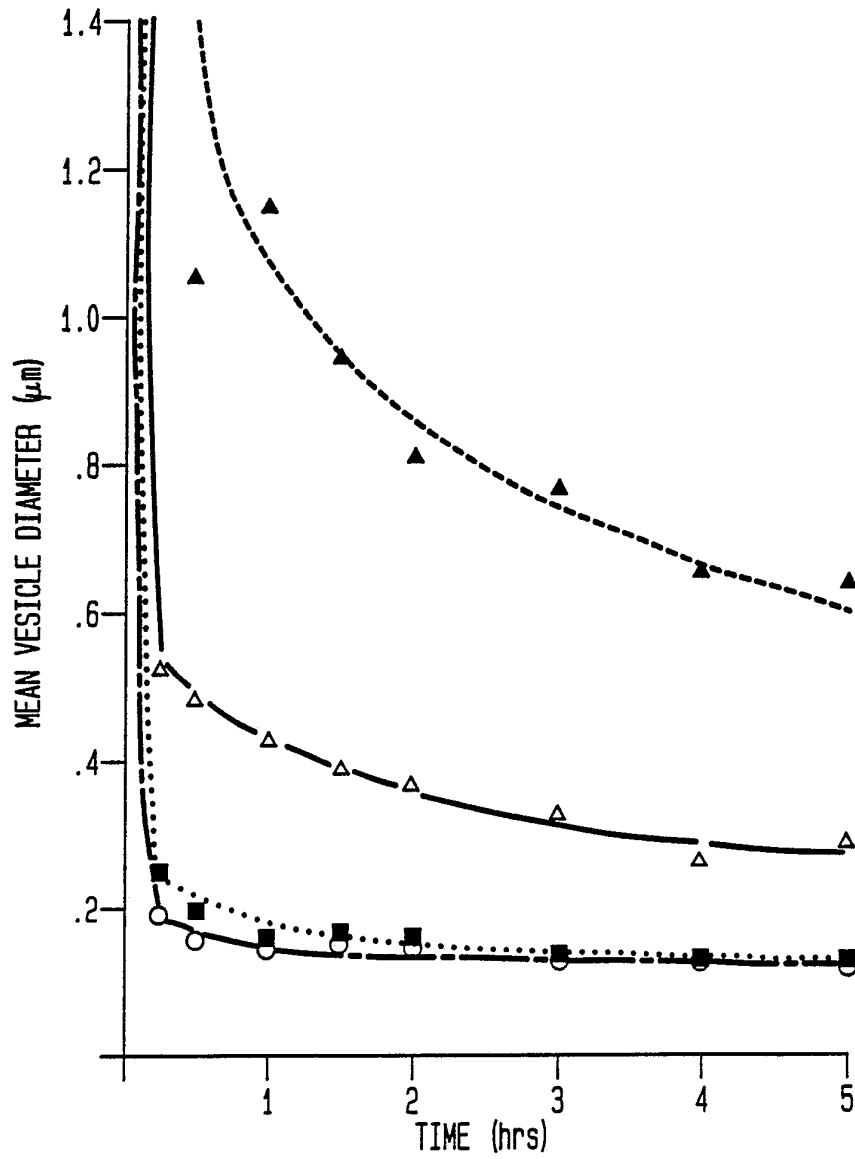
20

25

30

35

FIG. 1



SUBSTITUTE SHEET



FIG. 2

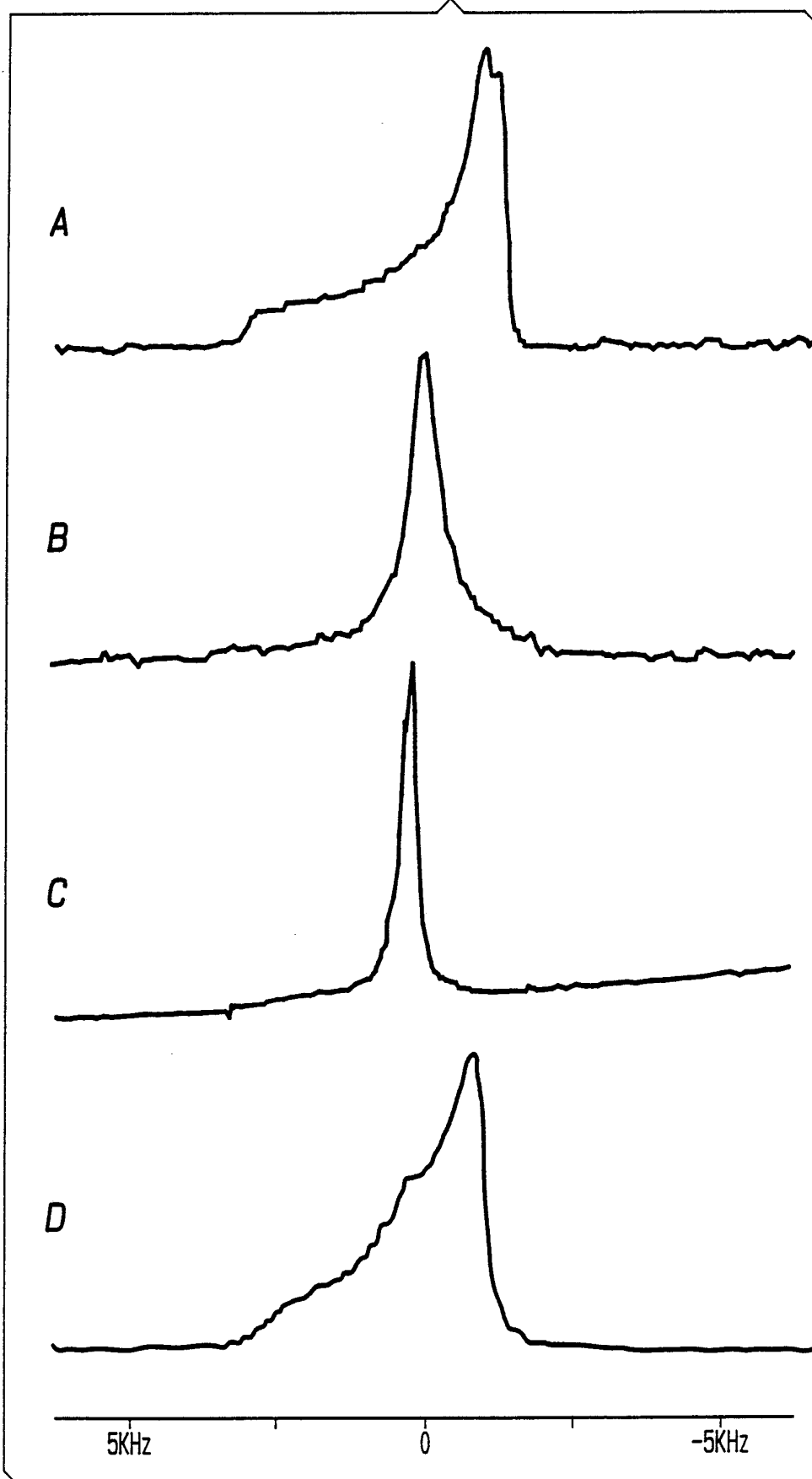
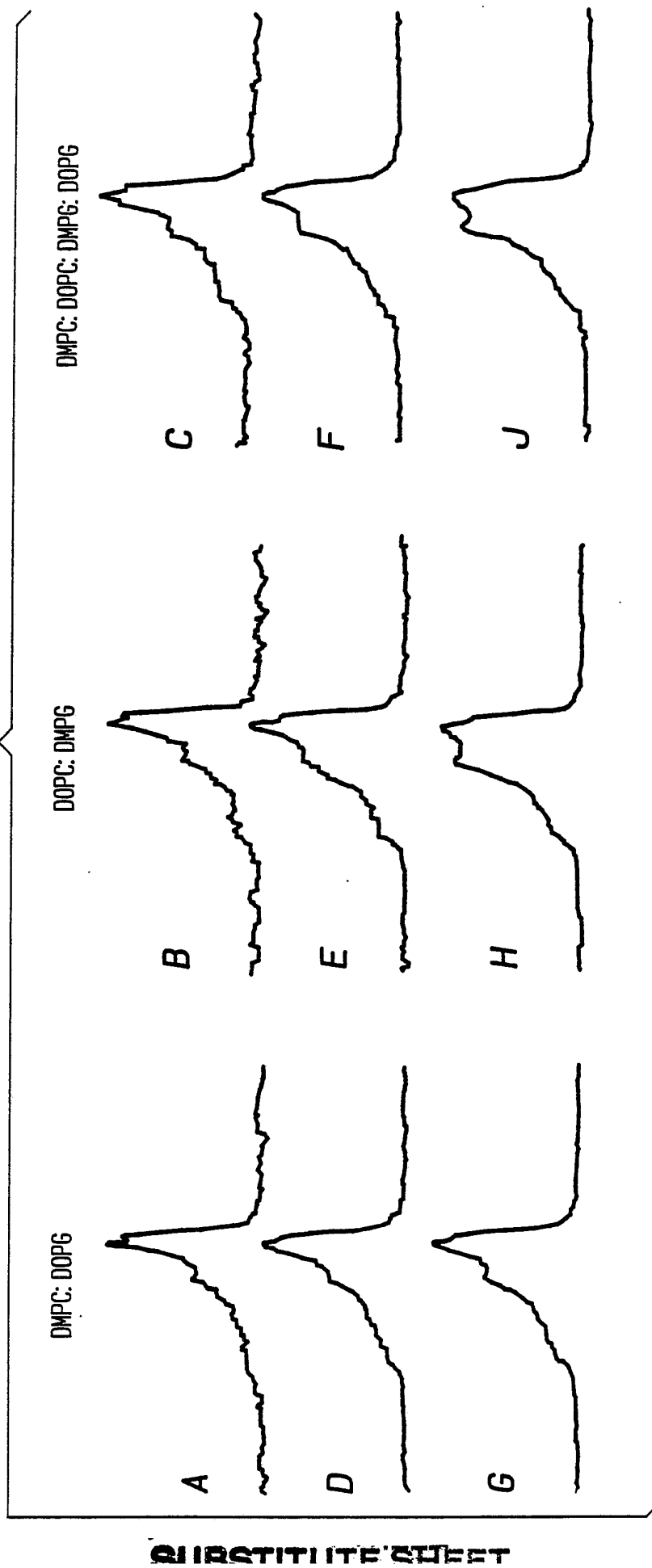


FIG. 3



BIOPHILITE

# INTERNATIONAL SEARCH REPORT

International Application No. PCT/US88/04632

<b>I. CLASSIFICATION OF SUBJECT MATTER</b> (if several classification symbols apply, indicate all) <sup>6</sup>		
According to International Patent Classification (IPC) or to both National Classification and IPC INT. CL. (4) A61K 9/66, 37/22; B01J 13/02 U.S. CL. 264/4.1, 4.3; 424/450; 436/829		
<b>II. FIELDS SEARCHED</b>		
Minimum Documentation Searched <sup>7</sup>		
Classification System	Classification Symbols	
U.S. CL.	264/4.1, 4.3; 424/450; 436/829.	
Documentation Searched other than Minimum Documentation to the Extent that such Documents are Included in the Fields Searched <sup>8</sup>		
<b>III. DOCUMENTS CONSIDERED TO BE RELEVANT</b> <sup>9</sup>		
Category *	Citation of Document, <sup>11</sup> with indication, where appropriate, of the relevant passages <sup>12</sup>	Relevant to Claim No. <sup>13</sup>
$\frac{X}{Y}, P$	US, A, 4,762,720 JIZOMOTO PUBLISHED 09 AUGUST 1988 SEE ABSTRACT; COL. 1, LINE 62-COL.2, LINE 7; AND EXAMPLES.	<u>1, 7, 8, 11</u> 2-6, 9, 10,12
Y	US, A, 4,515,736 DEAMER PUBLISHED 07 MAY 1985 SEE COL. 3, LINES 8-40, ESP. LINES 20, 21, AND 29 AND COL. 4, LINE 48-COL. 5, LINE 4.	2-6, 9, 10,12
X	US, A, 4,673,567 JIZOMOTO PUBLISHED 16 JUNE 1987 SEE EXAMPLES 1-5, 7 AND 8.	1, 7, 8
A	US,A, 4,310,505 BALDESCHWIELER ET AL PUBLISHED 12 JANUARY 1982.	1-12
A	US, A, 4,619,794 HAUSER PUBLISHED 28 OCTOBER 1986.	1-12
A	PROC. NATL.ACAD,SCI. USA, VOL. 79, PAGES 1683-1687, MARCH 1982, BIOCHEMISTRY, HAUSER ETAL., "SPONTANEOUS VESICULATION OF PHOSPHOLIPIDS: A SIMPLE AND QUICK METHOD OF FORMING UNILAMELLAR VESICLES".	1-12
<p>* Special categories of cited documents: <sup>10</sup></p> <p>"A" document defining the general state of the art which is not considered to be of particular relevance</p> <p>"E" earlier document but published on or after the international filing date</p> <p>"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)</p> <p>"O" document referring to an oral disclosure, use, exhibition or other means</p> <p>"P" document published prior to the international filing date but later than the priority date claimed</p> <p>"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention</p> <p>"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step</p> <p>"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.</p> <p>"&amp;" document member of the same patent family</p>		
<b>IV. CERTIFICATION</b>		
Date of the Actual Completion of the International Search	Date of Mailing of this International Search Report	
10 MARCH 1989	<b>18 APR 1989</b>	
International Searching Authority	Signature of Authorized Officer	
ISA/US	<i>Richard D. Lovering</i> Richard D. Lovering	