



US006576011B2

(12) **United States Patent**
Portney

(10) **Patent No.:** **US 6,576,011 B2**
(45) **Date of Patent:** ***Jun. 10, 2003**

- (54) **MULTIFOCAL OPHTHALMIC LENS**
 - (75) Inventor: **Valdemar Portney**, Irvine, CA (US)
 - (73) Assignee: **Advanced Medical Optics, Inc.**, Santa Ana, CA (US)
 - (*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 36 days.
- This patent is subject to a terminal disclaimer.

EP	0351471	1/1990
GB	939016	10/1963
GB	2058391 A	4/1981
GB	2129155 A	5/1984
GB	2146791 A	4/1985
GB	2192291	1/1988
WO	WO87/00299	1/1987
WO	WO86/03961	12/1987
WO	WO87/07496	12/1987
WO	8902251	3/1989
WO	8911672	11/1989
WO	9000889	2/1990
ZA	888414	11/1988

OTHER PUBLICATIONS

- (21) Appl. No.: **09/792,893**
- (22) Filed: **Feb. 26, 2001**
- (65) **Prior Publication Data**

US 2001/0008977 A1 Jul. 19, 2001

Related U.S. Application Data

- (62) Division of application No. 09/221,558, filed on Dec. 28, 1998, now Pat. No. 6,221,105, which is a division of application No. 08/885,987, filed on Jun. 30, 1997, now Pat. No. 5,919,229, which is a division of application No. 08/592,752, filed on Jan. 26, 1996, now Pat. No. 5,702,440.
- (51) **Int. Cl.⁷** **A61F 2/16**
- (52) **U.S. Cl.** **623/6.28**
- (58) **Field of Search** 623/FOR 105, 623/6.23-6.24, 6.27-6.29, 5.11-5.16; 351/161

- (56) **References Cited**

U.S. PATENT DOCUMENTS

1,483,509 A	1/1924	Bugbee
2,129,305 A	9/1938	Feinbloom
2,274,142 A	2/1942	Houchin

(List continued on next page.)

FOREIGN PATENT DOCUMENTS

AU	3225789	10/1989
CA	159395	12/1914
DE	2702117	7/1978
EP	0140063	5/1985

IOL Technologie Brochure, MF4 The Autofocus Lens, 1995 (6 pages).
 "Lens Design Fundamentals"; R. Kingslake; Institute of Optics University of Rochester, Rochester, NY; Academic Press 1978; pp. 36-39.
 Jan. 1988 Article: Contact Lens Practice.
 Sep. 1960 Article: Encyclopedia of Contact Lens Practice.
 Jun. 1960 Article: Further Developments of Bifocal Contact Lenses pp. 185-186, Contacto, The Contact Lens Journal (1959).
 "The Shah Bifocal Intraocular Lens Implant", Shah & Shah Intraocular Lens Laboratories, Calcutta, India.
 "A Three-Part System For Refining Intraocular Lens Power Calculations", *Journal of Cataract and Refractive Surgery*, J.T. Holladay, M.D., et al, vol. 14, Jan. 1988, pp. 17-23.

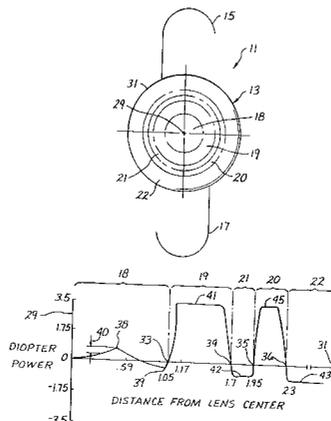
Primary Examiner—David H. Willse

(74) *Attorney, Agent, or Firm*—Frank Uxa; Peter Jon Gluck

(57) **ABSTRACT**

A multifocal ophthalmic lens, having outer annular zones with vision correction powers less than a far vision correction power of the patient, is disclosed. These additional annular zones come into play, when the pupil size increases under dim lighting conditions, to thereby compensate for the near-vision powered annular zones. The net effect of the additional near vision annular zones and the additional annular zones having power less than the far vision correction power is to shift the best quality image from in front of the retina to an area on the retina of the eye, to thereby reduce halo effects and improve image contrast.

7 Claims, 2 Drawing Sheets



U.S. PATENT DOCUMENTS					
			4,618,229 A	10/1986	Jacobstein et al.
			4,636,049 A	1/1987	Blaker
			4,636,211 A	1/1987	Nielsen et al.
			4,637,697 A	1/1987	Freeman
			4,641,934 A	2/1987	Freeman
			4,693,572 A	9/1987	Tsuetaki et al.
			4,704,016 A	11/1987	de Carle
			4,720,286 A	1/1988	Bailey et al.
			4,752,123 A	6/1988	Blaker
			4,759,762 A	7/1988	Grendahl
			4,769,033 A	9/1988	Nordan
			4,813,955 A	3/1989	Achatz et al.
			4,830,481 A	5/1989	Futhey et al.
			4,881,804 A	11/1989	Cohen
			4,890,912 A	1/1990	Visser
			4,890,913 A	1/1990	De Carle
			4,898,461 A	2/1990	Portney
			4,906,246 A	3/1990	Grendahl
			4,917,681 A	4/1990	Nordan
			4,919,663 A	4/1990	Grendahl
			4,921,496 A	5/1990	Grendahl
			4,923,296 A	5/1990	Erickson
			4,938,583 A	7/1990	Miller
			4,976,534 A	12/1990	Miege
			4,983,181 A	* 1/1991	Civerchia 623/5.11
			5,000,559 A	3/1991	Takahashi et al.
			5,002,382 A	3/1991	Seidner
			5,019,099 A	5/1991	Nordan
			5,089,024 A	2/1992	Christie et al.
			5,096,285 A	3/1992	Silberman
			5,112,351 A	5/1992	Christie et al.
			5,152,786 A	* 10/1992	Hanna 623/5.11
			5,166,711 A	11/1992	Portney
			5,192,317 A	3/1993	Kalb
			5,225,858 A	7/1993	Portney
			5,270,744 A	12/1993	Portney
			5,682,223 A	10/1997	Menezes et al.
					* cited by examiner
2,405,989 A	8/1946	Beach			
2,511,517 A	6/1950	Speigel			
3,004,470 A	10/1961	Ruhle			
3,031,927 A	5/1962	Wesley			
3,034,403 A	5/1962	Neeffe			
RE25,286 E	11/1962	DeCarle			
3,210,894 A	10/1965	Bentley			
3,227,507 A	1/1966	Feinbloom			
3,339,997 A	9/1967	Wesley			
3,420,006 A	1/1969	Barnett			
3,431,327 A	3/1969	Tsuetaki			
3,482,906 A	12/1969	Volk			
3,542,461 A	11/1970	Girard et al.			
3,693,301 A	9/1972	Lemaltre			
3,794,414 A	2/1974	Wesley			
3,932,148 A	1/1976	Krewalk, Sr.			
4,055,378 A	10/1977	Feneberg et al.			
4,062,629 A	12/1977	Winthrop			
4,073,579 A	2/1978	Deeg et al.			
4,195,919 A	4/1980	Shelton			
4,199,231 A	4/1980	Evans			
4,210,391 A	7/1980	Cohen			
4,240,719 A	12/1980	Guilino et al.			
4,274,717 A	6/1981	Davenport			
4,307,945 A	12/1981	Kitchen et al.			
4,315,673 A	2/1982	Guilino et al.			
4,338,005 A	7/1982	Cohen			
4,340,283 A	7/1982	Cohen			
4,346,482 A	* 8/1982	Tennant et al. 623/5.15			
4,377,329 A	3/1983	Poler			
4,402,579 A	9/1983	Poler			
4,418,991 A	12/1983	Breger			
4,504,982 A	3/1985	Burk			
4,573,775 A	3/1986	Bayshore			
4,580,882 A	4/1986	Nuchman et al.			
4,596,578 A	6/1986	Kelman			
4,618,228 A	10/1986	Baron et al.			

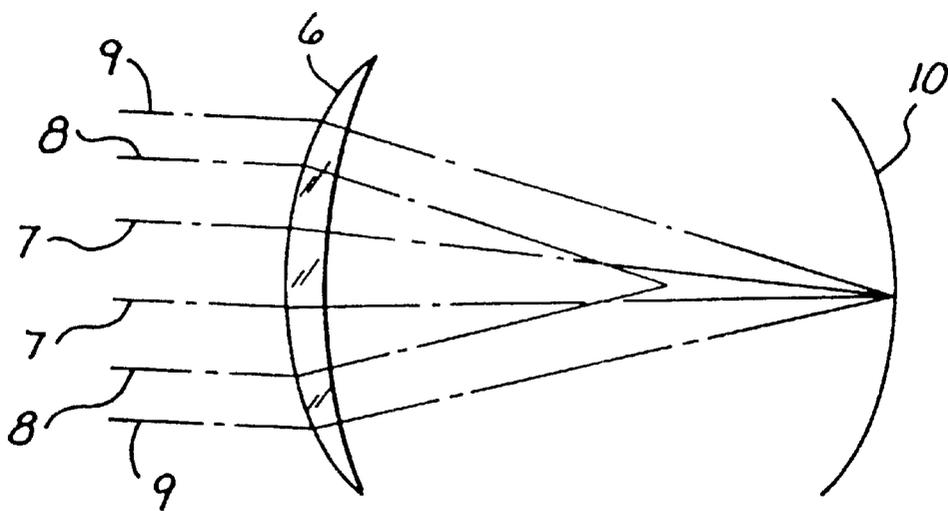


Fig. 1
PRIOR ART

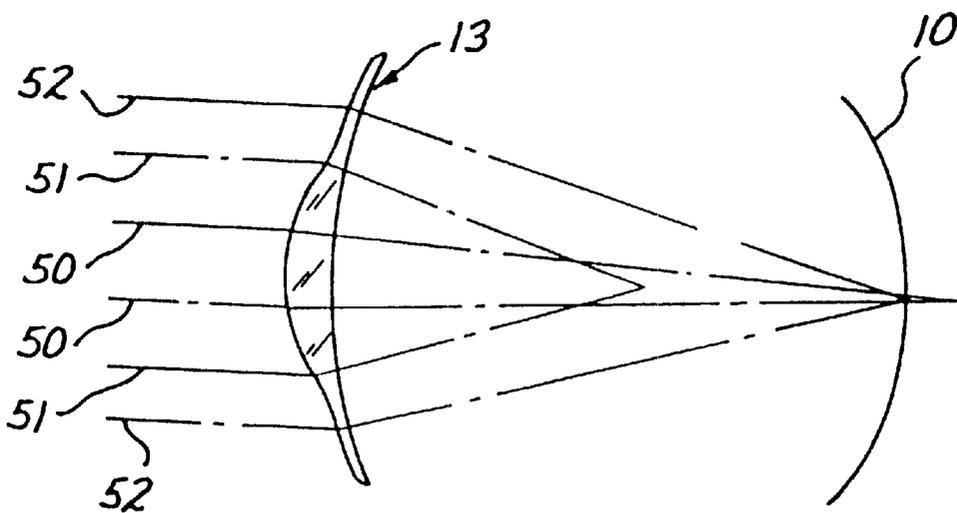


Fig. 5

Fig. 2

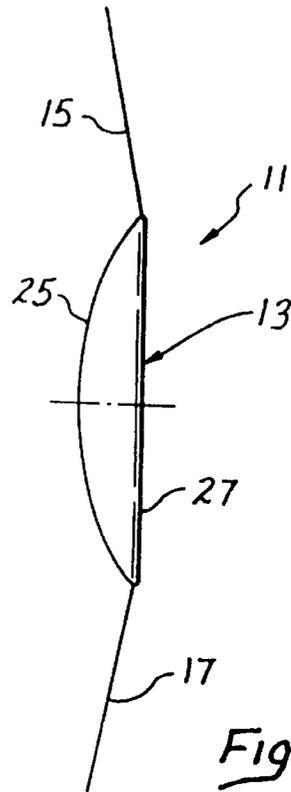
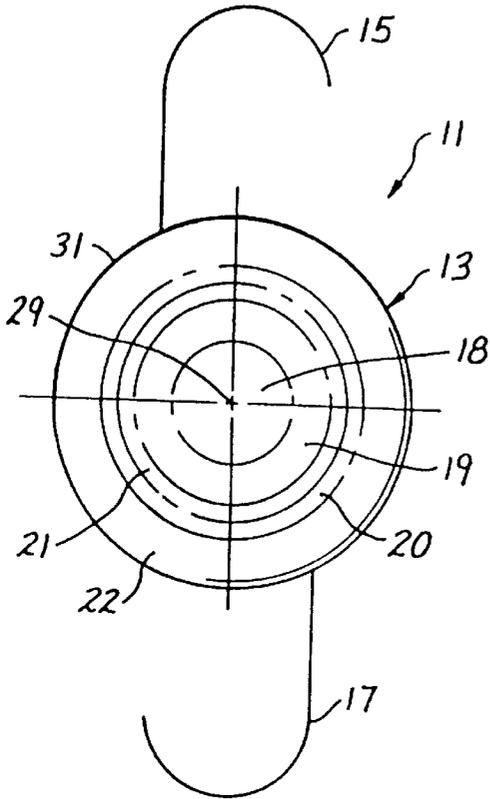


Fig. 3

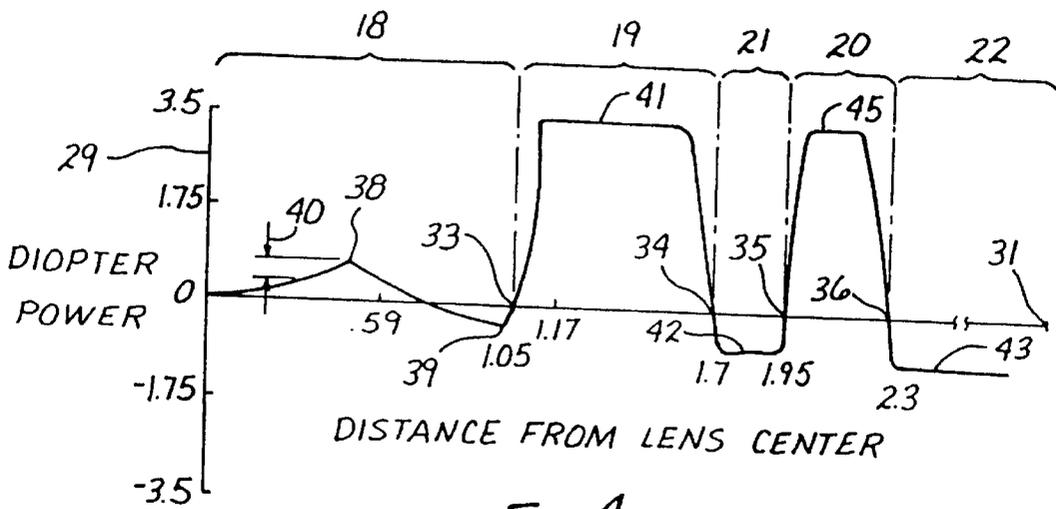


Fig. 4

MULTIFOCAL OPHTHALMIC LENS

This is a division of application Ser. No. 09/221,558, filed Dec. 28, 1998, now U.S. Pat. No. 6,221,105, which is a division of application Ser. No. 08/885,987 filed Jun. 30, 1997, now U.S. Pat. No. 5,919,229, which is a division of application Ser. No. 08/592,752 filed Jan. 26, 1996, now U.S. Pat. No. 5,702,440.

FIELD OF THE INVENTION

The present invention relates generally to ophthalmic lenses and, more particularly, to a multifocal ophthalmic lens adapted for implantation in an eye, such as an intraocular lens, or to be disposed in a cornea, such as a corneal inlay.

BACKGROUND OF THE INVENTION

The general construction of a multifocal ophthalmic lens is known in the art. U.S. Pat. No. 5,225,858, which is incorporated herein by reference, discloses a multifocal ophthalmic lens including a central zone circumscribed by multiple concentric, annular zones. This patent discloses a means of providing improved image quality and light intensity for near images. The improved image quality is accomplished by maintaining the near vision correction power of appropriate zones of the lens substantially constant for a major segment of the near vision correction power region of each zone, and by providing a central zone having an increased depth of focus.

The major segment of each near vision correction power region, which has a substantially constant near vision correction power, inherently reduces the depth of focus associated with far vision. The location of near focus is typically immaterial for near vision, because of the ability of the user to easily adjust the working distance of the target object. The patent discloses progressive vision correction powers in the central zone for extending the depth of focus. The increased depth of focus provided by the central zone helps to compensate for the reduction in depth of focus associated with the near vision correction power regions. This feature is particularly applicable to an intraocular lens, since the patient has minimal residual accommodation, i.e., the ability of a normal eye to see objects at different distances.

FIG. 1 shows how the multifocal ophthalmic lens 6 of the prior art focuses parallel incoming light onto the retina 10 of the eye. For the normal lighting condition with a 3 mm pupil diameter, the rays 7 pass through a far focus region of the multifocal ophthalmic lens 6, and are focused onto the retina 10. The rays 8 pass through a near region of the multifocal ophthalmic lens 6, and are focused into a region between the retina 10 and the multifocal ophthalmic lens 6.

The multifocal ophthalmic lens 6 shown in FIG. 1 shows the passage of parallel rays through the multifocal ophthalmic lens 6 in a well-lit environment. In low lighting conditions, the pupil enlarges, and additional annular zones of the multifocal ophthalmic lens 6 become operative to pass light therethrough. These additional annular regions operate to provide additional far (rays 10 in FIG. 1) and near-focus corrective powers to the multifocal ophthalmic lens 6. Presence of the additional intermediate and near rays shift the best image quality for far vision to the location in front of the retina. As a result, in low lighting conditions the best quality image of the multifocal ophthalmic lens 6 appears in a region slightly in front of the retina 7. A user looking through the multifocal ophthalmic lens 6 while driving at night, for example, may notice an undesirable halo affect around a bright source of light. The shift in the best quality

image just in front of the retina 7 instead of on the retina 7 increases the halo effect making driving for some people difficult.

A problem has thus existed in the prior art of providing a multifocal ophthalmic lens, which can provide a desirable far vision correction in low lighting conditions, but which does not unnecessarily elevate halos and contrast reductions under increased pupil size which usually occurs in low lighting conditions. Thus, the prior art has been unable to produce a multifocal ophthalmic lens, which achieves a best quality image on the retina (instead of slightly in front of the retina) in low lighting conditions.

Under low lighting conditions, the best quality image of prior art multifocal ophthalmic lenses is not focused on the retina of the eye. Instead, these prior art multifocal ophthalmic lenses have a best quality image in front of the retina in low lighting conditions, which corresponds to a mean power of the multifocal ophthalmic lens being slightly higher than the far vision correction power required for the patient.

SUMMARY OF THE INVENTION

As light diminishes and pupil size correspondingly increases, the outer annular zones of a multifocal ophthalmic lens begin to pass light therethrough. These outer annular zones traditionally introduce additional near vision correction power, which effectively shifts the best quality image from on the retina to an area slightly in front of the retina.

The outer annular zones of the present invention have vision correction powers, which are less than the far vision correction power of the patient, to compensate for the increase in the mean power of the multifocal ophthalmic lens. A multifocal ophthalmic lens, having outer annular zones with vision correction powers less than a far vision power of the patient, is disclosed. The additional annular zone or zones come into play when the pupil size increases under dim lighting conditions, to thereby compensate for the additional near vision annular zones introduced by the enlarged pupil size. The net effect of the additional near vision annular zones and the additional annular zones having power less than the far vision correction power is to focus the best quality image onto the retina of the eye, to thereby reduce halo effects and improve contrast.

The multifocal ophthalmic lens of the present invention is adapted to be implanted into an eye or to be disposed in a cornea, and has a baseline diopter power for far vision correction of the patient. The multifocal ophthalmic lens includes a central zone having a mean vision correction power equivalent to or slightly greater than the baseline diopter power depending upon pupil size, and includes a first outer zone located radially outwardly of the central zone.

A second outer zone located radially outwardly of the first outer zone provides vision correction power, that is less than the baseline diopter power. The vision correction power of the second outer zone can be substantially constant. Light generally does not pass through the second outer zone under bright lighting conditions.

A third outer zone of the multifocal ophthalmic lens comes into play in lower lighting conditions, and includes a vision correction power greater than the baseline diopter power. A fourth outer zone circumscribes the third outer zone, and includes a vision correction power, that is less than the baseline diopter power. This fourth outer zone passes light in very low lighting conditions, when the pupil is significantly dilated. The second and fourth outer zones serve to focus light slightly behind the retina of the eye, to

thereby compensate for light focused in front of the retina of the eye by the first and third outer zones, under dim lighting conditions.

BRIEF DESCRIPTION OF THE PREFERRED EMBODIMENTS

FIG. 1 is a schematic view illustrating the focusing of light of a prior art multifocal ophthalmic lens onto a retina;

FIG. 2 is a plan view of an intraocular multifocal ophthalmic lens of the presently preferred embodiment;

FIG. 3 is a side elevational view of the intraocular multifocal ophthalmic lens of the presently preferred embodiment;

FIG. 4 is a plot of the power of the optic versus distance from the optic axis for the intraocular multifocal ophthalmic lens of the presently preferred embodiment;

FIG. 5 is a schematic view illustrating the focusing of light of the intraocular multifocal ophthalmic lens of the presently preferred embodiment onto a retina.

These and other aspects of the present invention are apparent in the following detailed description and claims, particularly when considered in conjunction with the accompanying drawings in which like parts bear like reference numerals.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

FIGS. 2 and 3 show an intraocular lens 11, which comprises a circular optic 13 and two fixation members 15 and 17. The optic 13 may be constructed of rigid biocompatible materials, such as polymethylmethacrylate (PMMA), or flexible, deformable materials, such as silicone, hydrogel and the like which enable the optic to be rolled or folded for insertion through a small incision into the eye.

In the presently preferred embodiment, the fixation members 15 and 17 are fine hair-like strands or filaments which are attached to the optic 13 using conventional techniques. The fixation members 15 and 17 may be constructed of a suitable polymeric material, such as PMMA or polypropylene. Alternatively, the fixation members 15 and 17 may be integral with the optic 13. The optic 13 and the fixation members 15 and 17 may be of any desired number and configuration, and the configurations illustrated are purely illustrative.

The optic 13 has a central zone 18, inner and outer annular near zones 19 and 20, and an annular far zones 21 and 22. In the presently preferred embodiment, the central zone 18 is circular, and the peripheries of the annular zones 19-22 are circular. The annular zones 19-22 circumscribe the central zone 18, and the zones are contiguous. The zones 19-22 are concentric and coaxial with the optic 13.

The zones 18-22 are used in describing the vision correction power of the optic 13, and they are arbitrarily defined. Thus, the peripheries of the zones 18-22 and the number of zones may be selected as desired. However to facilitate describing the optic 13, the peripheries of the annular zones 19-22 are considered to be the zero crossings in FIG. 4. Although the boundaries of the zones 18-22 are indicated by phantom lines in FIG. 2, it should be understood that the optic 13 has no such lines in any of its surfaces and that these lines constitute reference lines which define the zones.

As shown in FIG. 3, the optic 13 has a convex anterior surface 25 and a planar posterior surface 27; however, these configurations are merely illustrative. Although the vision

correction power may be placed on either of the surfaces 25 and 27, in the presently preferred embodiment, the anterior surface 25 is appropriately shaped to provide the desired vision correction powers.

FIG. 4 shows the preferred manner in which the vision correction power of the optic 13 varies from the center or optical axis 29 of the optic 13 to the circular outer periphery 31 of the optic. A preferred power distribution curve for a corneal inlay may be similar, or identical, to the curve of FIG. 4.

In FIG. 4, the vertical or "Y" axis represents the variation in diopter power of the optic 13 from the baseline or far vision correction power, and the "X" or horizontal axis shows the distance outwardly from the optical axis 29 in millimeters. Thus, the zero-diopter or baseline power of FIG. 4 is the power required for far vision for a conventional mono-focal intraocular lens. The power variation shown in FIG. 4 is applicable to any radial plane passing through the optical axis 29. In other words, the power at any given radial distance from the optical axis 29 is the same.

The central zone 18 extends from the optical axis 29 to a circular periphery 33, the first annular near zone 19 is considered as extending from the periphery 33 to a circular periphery 34, and the outer annular near zone 20 is considered as extending from a periphery 35 to a periphery 36. The negative diopter power of the two zones 21, 22 are of less power than required for far vision and may be considered as far, far vision correction powers. The annular far, far zone 21 extends between the peripheries 34 and 35, and the annular far, far zone 22 extends from the periphery 36 radially outwardly to the outer periphery 31 of the optic 13. As shown in FIG. 4, the vision correction power crosses the "X" axis or baseline at the peripheries 33, 34, 35 and 36.

As shown in FIG. 4, the vision correction power varies progressively and continuously from a baseline diopter power at the optical axis 29 to an apex 38 and then decreases continuously and progressively from the apex 38 back through the baseline diopter power to a negative diopter power at a point 39. From the point 39, the vision correction power increases continuously and progressively through the periphery 33 into the inner annular near zone 19. Of course, the diopters shown on the ordinate in FIG. 4 are merely exemplary, and the actual correction provided will vary with the prescription needs of the patient.

The apex 38 has a vision correction power for intermediate vision. The intermediate vision correction powers may be considered as being in a zone 40 which may be between 0.5 and 0.75 diopters from the baseline diopter power, as presently embodied. The far vision correction powers may be considered as lying between the zone 40 and the baseline diopter correction, and the far, far vision correction powers are negative. The intermediate, far, and far, far powers combine to provide a mean power in the central zone 18.

Within the inner annular near zone 19, the vision correction power varies continuously and progressively from the periphery 33 to a plateau 41; and from the plateau 41, the vision correction power varies continuously and progressively back to the periphery 34 at the baseline.

In the far, far zone 21 the vision correction power is below the far zone correction power, and is substantially constant. This vision correction power returns to the baseline at the periphery 35.

In the outer annular near zone 20, the power varies continuously and progressively from the periphery 35 to a plateau 45, and returns continuously and progressively from the plateau 45 to the baseline at the periphery 36.

In the far, far zone **22**, the vision correction power is substantial constant, below the baseline vision correction power. The substantially constant vision correction power of the far, far zone **22** is slightly lower than the substantially constant vision correction power of the far, far zone **21**, as presently embodied. The vision correction power of the far, far zone **22** remains negative from the periphery **36** to the baseline correction power at the outer periphery **31**.

The inner near zone **19** has regions adjacent the peripheries **33** and **34** with far vision correction powers and a second region, which includes the plateau **41**, with near vision correction powers. Similarly, the outer near zone **20** has regions adjacent the peripheries **35** and **36** with far vision correction powers and a second region, which includes the plateau **45**, with near vision correction powers. For example, the near vision powers may be those which are above 2 or 2.5 diopters. The 2 to 2.5 diopters correspond to about 20 to 15 inches, respectively, of working distance, and this distance corresponds to the beginning of near activities. The two far, far vision correction plateaus **42**, **43** of the two far, far annular zones **21**, **22**, respectively, preferably comprise diopter powers approximately one fifth of the distance between the baseline and the plateaus **41**, **45**, but located below the baseline.

As shown in FIG. 4, each of these "near" regions has a major segment, i.e., the plateaus **41** and **45** in which the near vision correction power is substantially constant. The plateau **41**, which lies radially inwardly of the plateau **45**, has a greater radial dimension than the plateau **45**. The difference in radial dimension of the plateaus **41** and **45** allows these two plateaus to have approximately the same area.

Only a relatively small portion of the anterior surface **25** (FIG. 3) is dedicated to intermediate vision powers. This can be seen by the relatively small radial region which corresponds to the intermediate zone **40** (FIG. 4) and by the rapid change in diopter power between the plateaus **41** and **45** and the baseline diopter axis.

The diagrammatic view of FIG. 5 shows how the multifocal ophthalmic lens **13** of the present invention focuses parallel light onto a retina **10** of the eye, in dim lighting conditions. The parallel rays **50** pass through the central portion **18** of the multifocal ophthalmic lens **13**, and are focused onto the retina **10**. The rays **51** pass through the intermediate focus region **40** of the central zone **18**, and are focused in an area between the retina **10** and the multifocal ophthalmic lens **13**. The rays **52** pass through the plateau **41** of the near zone **19** and, depending upon the lighting conditions, pass through the plateaus **42**, **43** of the two far, far zones **21**, **22**, and the plateau **45** of the near zone **20**. These rays **52** are focused slightly behind the retina **10**. In the presently preferred embodiment, the distance at which the rays **52** are focused behind the retina **10**, is approxi-

mately one-fifth of the distance at which the rays **51** are focused in front of the retina **10**. The combination of the rays **50**, **51**, and **52** combine to form a best quality image on the retina **10** in dim lighting conditions.

While this invention has been described with respect to various specific examples and embodiments, it is to be understood that the invention is not limited thereto and that it can be variously practiced within the scope of the following claims.

What is claimed is:

1. A multifocal intraocular lens for providing vision correction power, the multifocal intraocular lens having a central optical axis, an outer periphery and a baseline diopter power for far vision correction, the multifocal intraocular lens being sized and structured to be implanted in an eye, and comprising:

a central zone having a vision correction power at the central optical axis no less than the baseline diopter power and a vision correction power approximately equal to or greater than the baseline diopter power, the central zone having a progressive power region in which the vision correction power varies progressively;

a first zone having a near vision correction power, the first zone being located radially outwardly of the central zone; and

a second zone located radially outwardly of the first zone and extending to the outer periphery of the multifocal intraocular lens and having a vision correction power less than the baseline diopter power substantially throughout the second zone.

2. The multifocal intraocular lens according to claim 1, wherein the first zone is annular and circumscribes the central zone, and the second zone is annular and circumscribes the first zone.

3. The multifocal intraocular lens according to claim 1, wherein the vision correction power of the second zone is substantially constant throughout.

4. The multifocal intraocular lens according to claim 2, wherein the vision correction power of the second zone is substantially constant throughout.

5. The multifocal intraocular lens according to claim 1, wherein the vision correction power at the central optical axis is approximately the baseline diopter power.

6. The above-identified application has been carefully reviewed claim 5, wherein the first zone is annular and circumscribes the central zone, and the second zone is annular and circumscribes the first zone.

7. The multifocal intraocular lens according to claim 5, wherein the vision correction power of the second zone is substantially constant throughout.

* * * * *