

(19) World Intellectual Property  
Organization  
International Bureau



(43) International Publication Date  
22 July 2004 (22.07.2004)

PCT

(10) International Publication Number  
**WO 2004/060157 A1**

(51) International Patent Classification<sup>7</sup>: **A61B 5/06**, 6/12

(21) International Application Number:  
PCT/IB2003/006233

(22) International Filing Date:  
19 December 2003 (19.12.2003)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:  
03100011.0 7 January 2003 (07.01.2003) EP

(71) Applicant (for DE only): **PHILIPS INTELLECTUAL  
PROPERTY & STANDARDS GMBH** [DE/DE]; Stein-  
damm 94, 20099 Hamburg (DE).

(71) Applicant (for all designated States except DE, US):  
**KONINKLIJKE PHILIPS ELECTRONICS N.V.**  
[NL/NL]; Groenewoudseweg 1, NL-5621 BA Eindhoven  
(NL).

(72) Inventors; and

(75) Inventors/Applicants (for US only): **SABCZYNSKI, Jo-  
erg** [DE/DE]; c/o Philips Intellectual Property & Standards

GmbH, Weissshausstr. 2, 52066 Aachen (DE). **RASCHE,  
Volker** [DE/DE]; c/o Philips Intellectual Property & Stan-  
dards GmbH, Weissshausstr. 2, 52066 Aachen (DE).

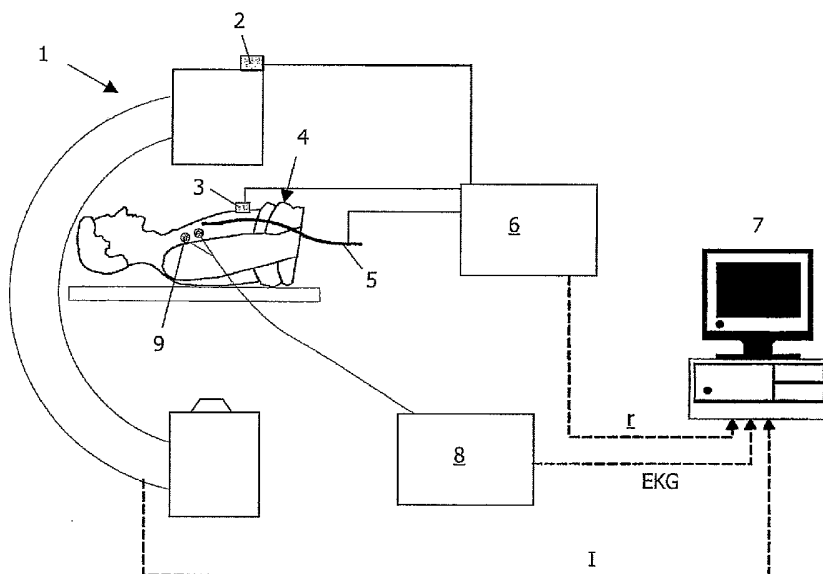
(74) Agent: **VOLMER, Georg**; Philips Intellectual Property &  
Standards GmbH, Weissshausstr. 2, 52066 Aachen (DE).

(81) Designated States (national): AE, AG, AL, AM, AT, AU,  
AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR,  
CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD,  
GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR,  
KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN,  
MW, MX, MZ, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU,  
SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA,  
UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.

(84) Designated States (regional): ARIPO patent (BW, GH,  
GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW),  
Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM),  
European patent (AT, BE, BG, CH, CY, CZ, DE, DK, EE,  
ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PT, RO, SE,  
SI, SK, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA,  
GN, GQ, GW, ML, MR, NE, SN, TD, TG).

[Continued on next page]

(54) Title: METHOD AND ARRANGEMENT FOR TRACKING A MEDICAL INSTRUMENT



(57) Abstract: The invention relates to a method and an arrangement for the intravascular or intracardial navigation of a catheter (5). Using an X-ray fluoroscopy device (1), firstly an image database of 2D images is generated, where at the same time as each 2D image (I) is taken the associated heartbeat phase is recorded using an ECG (8). During the catheter intervention, the position of the catheter (5) is measured by means of a position measurement unit (6), and at the same time the ECG and preferably also a signal that is dependent on the breathing movement are recorded. The current spatial position of the catheter (5) that is measured is then assigned the 2D image of the image database which corresponds in terms of the heartbeat phase and also possibly in terms of the breathing phase, on which image the position of the catheter can be represented.

WO 2004/060157 A1



**Published:**

— *with international search report*

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## Method and arrangement for tracking a medical instrument

The invention relates to a method of tracking a medical instrument that is inserted into the body of a patient, and to an arrangement that is suitable for carrying out the method.

5

An arrangement and a method of the type mentioned above are known from DE 199 46 948 A1. In said document, prior to a catheter investigation, an image database having a number of three-dimensional images of a periodically moving organ of the body, such as for example of the heart, is generated, where a movement signal of the organ of the body is recorded at the same time as the images are taken. The movement signal may be, in particular, an electrocardiogram (ECG) and/or a breathing movement signal. During the subsequent medical intervention, the spatial position of the instrument, and also of a reference probe, is determined by a position measurement unit, and at the same time the movement signal is recorded. Using the movement signal, it is then possible for the 3D image that corresponds in terms of the movement phase of the organ of the body to be selected from the image database. Using the position of the reference probe, which is known in this 3D image, it is then possible to determine the current spatial position of the instrument relative to the 3D image, and to represent it, for example, superposed on the 3D image. One disadvantage of the known method is the high expenditure associated therewith. For instance, the three-dimensional images of the organ of the body first have to be produced using X-ray computer tomography or magnetic resonance imaging, and this does not only take a great deal of time but also greatly modifies the conventional working procedures of a catheter laboratory, since the necessary imaging methods are not available in the catheter laboratory and thus the taking of the images requires an additional time-intensive step. Furthermore, the time-intensive 3D imaging methods generally do not permit real-time updating of the 3D image during the intervention.

In the light of this, it is an object of the invention to simplify the tracking of the position of an instrument, so that it can be integrated more easily with the working procedure of an investigation and preferably permits real-time updating of the images during the intervention.

5           This object is achieved by a method having the features of claim 1 and by an arrangement having the features of claim 11. Advantageous refinements are given in the subclaims.

          The method according to the invention for tracking an instrument that is inserted into the body of a patient, such as a catheter or catheter tip for example, comprises  
10   the following steps of:

          a) Detection of a movement signal which represents the movement phases of a periodic internal movement of the body. Significant examples of a periodic internal movement of the body are the heartbeat and breathing.

          b) Generation of 2D images of a patient body volume of interest, and storage  
15   of the 2D images in an image database, where the associated imaging parameters (e.g. projection direction, etc.) and the associated movement phase (in the simplest case directly expressed by the movement signal) are stored together with each 2D image during the taking of the 2D image.

          c) Measurement of the spatial position of the instrument and optionally also  
20   measurement of the spatial position of at least one reference probe, where the reference probe can be fitted in particular externally on the body of the patient and/or on a medical instrument, or can be fitted inside the patient using a reference catheter or another medical instrument.

          d) Selection of at least one 2D image from the image database, which 2D  
25   image corresponds in terms of its associated movement phase to the movement phase at the time when the spatial position of the instrument was determined in step c).

          e) Determination of the position of the instrument on the 2D image selected in step d).

          The method has the advantage that the movement of the instrument is tracked  
30   using 2D images, which are produced anyway during the conventional procedure of medical (catheter) investigations. It is therefore seldom necessary to use additional equipment. On account of the simultaneous storage of imaging parameters, movement phases and 2D images in the image database, it is possible, during an operative intervention that is in progress, to represent the current spatial position of the instrument on that 2D image from the image

database which corresponds to the current movement phase. Displacements and changes in shape of organs of the body on account of periodic internal movements can in this way be taken into consideration or compensated for. Furthermore, movements of the patient as a whole or of the table on which the patient is lying can also be taken into consideration or compensated for.

An electrocardiogram and/or a breathing movement signal that is dependent on the breathing movement of the patient is preferably detected as a movement signal. Using these signals, it is possible to detect the most significant periodic internal movements in the body of a patient and thus to take these into consideration when determining the position of an instrument.

The position of the instrument which is determined in step e) is preferably represented superposed on the 2D images selected in step d). This makes it possible for the investigating physician to track the movement of the instrument directly on the 2D images.

According to a specific refinement of the method, only 2D images from a single movement phase are made available for selection from the image database in step d). This may in particular mean that the image database may even contain just a single 2D image. In this case, step d) of the method is reduced to ascertaining whether or not the only "selectable" movement phase corresponds to the movement phase of the current spatial position of the instrument. If the movement phases correspond to one another, the assignment can take place; otherwise, it must not take place. In this way, it is possible to reduce the representation frequency of the superposed representation of the instrument position and of the selected 2D image, and so an update of the current instrument position will only be represented when the movement phase thereof corresponds to the predefined movement phase of the 2D image. If the heartbeat is used as a basis for the periodic movement, the predefined 2D image can for example correspond to the end-systoles of the heartbeat, so that the superposed representation of the instrument on the 2D image is only refreshed at these points in the cardiac cycle. The computational outlay for the method can thereby be considerably reduced. By always using the same 2D image, a steady-state image background is established, and this facilitates visual tracking of the instrument.

According to another development of the method, step b) on the one hand (generation of 2D images for the image database) and steps c), d), e) on the other hand (measurement of the spatial position of the instrument; selection of at least one corresponding 2D image; determination of the position in the image) are carried out a number of times and in varying order. This means, in particular, that 2D images can be generated even while the

operative intervention is in progress, and this ensures that the image database which is used is always up-to-date.

Preferably, the image database contains 2D images from various projection directions. As a result, it is possible to represent the current spatial position of the instrument on various 2D images in parallel, or to select the best suited 2D image from a number of 2D images from a movement phase.

The 2D images are advantageously generated by means of X-radiation and/or ultrasound, so that the apparatus that is conventionally present during a catheter investigation can be used to produce them.

According to a development of the method, at least one reference probe is fitted on a movable X-ray device which is provided for generating the 2D images. The spatial position of the reference probe is then measured, according to steps b) and c) of the method, in parallel with the generation of the 2D images and with the determination of the spatial position of the instrument. Knowing the spatial position of the reference probe on the X-ray device makes it possible to determine the projection direction from the location of the X-ray device, without any additional apparatus being required. If another reference probe is additionally used on the patient, the projection direction can also be determined with respect to the patient.

Furthermore, using movement models of the body, it is possible to compensate for the breathing movement on the basis of the measured breathing positions.

The invention furthermore relates to an arrangement for tracking an instrument that is inserted into the body of a patient, which comprises the following elements:

a) A device for generating 2D images of a body volume of interest.  
b) A unit for determining the set imaging parameters of the device.  
c) A signal measurement unit for detecting a movement signal which represents the movement phases of a periodic internal movement of the body. As mentioned above, the internal movement of the body may in particular be the heartbeat and/or the breathing.

d) A storage unit for storing an image database of 2D images of the body volume together with the imaging parameters and the movement phases which belong to the respective 2D image.

e) A position measurement unit for measuring the spatial position of the instrument that is inserted into the body and optionally of at least one reference probe. The

position measurement unit may in particular comprise a transmitter for transmitting (modulated) electromagnetic fields and also a receiver for receiving these fields.

5 f) A control and computation unit for selecting at least one 2D image from the image database, which 2D image corresponds in terms of its associated movement phase to the movement phase belonging to the spatial position of the instrument, and for determining the position of the instrument on the selected 2D image.

Using the described arrangement, it is possible for the above-described method to be carried out so that its advantages can be achieved. In particular, it is important that the arrangement is compatible with a device such as is present as standard in conventional  
10 catheter investigations. In order to be able to represent the position of an instrument on the 2D image generated hereby, the arrangement comprises a unit for determining the set imaging parameters of the device. Knowledge thereof makes it possible subsequently to convert the measured spatial position of the instrument into a position on the selected 2D image.

15 Preferably, the arrangement is designed such that it is suitable for carrying out one or more variants of the method of the type described above. Thus, the signal measurement unit may in particular have means for measuring an electrocardiogram and/or for measuring the breathing movement of the patient. Furthermore, the device may in particular be an X-ray apparatus.

20

The invention will be further described with reference to examples of embodiments shown in the drawings to which, however, the invention is not restricted. The single figure schematically shows the components of an arrangement according to the  
25 invention.

Intravascular interventions are conventionally carried out in a catheter laboratory. Here, the operation field is observed fluoroscopically using an X-ray apparatus 1  
30 fitted on a C-arm. In coronary vessel disorders, a contrasting agent is conventionally applied locally, in order to show the vessel profile on the fluoroscopic image. In the course of therapeutic methods, such as a PTCA (Percutaneous Transluminal Coronary Angioplasty) for example, a catheter 5 is pushed into the target area, for example a stenosis in the heart of the patient 4, and its position is in turn monitored using X-ray fluoroscopy. This means that X-

ray fluoroscopy is used not only to show the anatomy of the patient but also to navigate the catheter to its target area. Therefore, the patient and the staff require additional doses of X-radiation which serve solely for navigation.

The arrangement shown in the figure allows, using the existing imaging apparatus of a catheter laboratory, navigation of the catheter 5 during cardiac or other intravascular interventions with a reduced amount of X-radiation. The overall system consists of

- a position measurement unit 6, such as for example an electromagnetic position measurement system (cf. DE 199 46 948 A1), which allows determination of the spatial position of the tip of the catheter 5 and also of a reference probe 3 on the patient 4 or of a reference probe 2 on the X-ray device 1 in a stationary coordinate system;
- a medical workstation (computer) 7, which receives the positions  $r$  determined by the position measurement unit 6, the electrocardiogram ECG from the ECG system 8, and the X-ray images I from the X-ray device 1;
- an X-ray fluoroscopy device 1 which is tracked and calibrated in terms of its setting by a reference probe 2;
- a tracked catheter 5 or guidewire;
- reference probes 3 on or in the patient;
- an ECG system 8 for taking an electrocardiogram using electrodes 9 attached to the patient.

Using such an arrangement, it is possible to navigate the catheter 5 in accordance with the following steps:

#### 1. Preoperative calibration phase:

During a calibration procedure, the imaging parameters of the fluoroscopic system 1 are determined. This calibration need be carried out only once, for example at the manufacturer's premises or during installation of the system 1 (see, for example, US 6 379 043, US 6 471 399).

#### 2. Image generation phase during the intervention:

2.1. Preparation: Preparation of the patient 4 including attachment of the ECG electrodes 9; fitting of the reference probes 3 for position tracking on the patient 4 (in the case of cardiac interventions on the thorax).

##### 2.2. Data gathering:

2.2.1. An X-ray image I or an image sequence is generated using the X-ray fluoroscopy system 1, where the anatomy of interest of the patient 4 is visible on the images.



2.2.2. For each image of the taken image sequence, additional information is recorded at the time it was taken, specifically, in particular, the current position of the C-arm of the X-ray fluoroscopy system 1, the current position of the reference probe(s) 3 on the patient and the associated ECG phase. The images and the aforesaid additional information  
5 form multimodal data.

2.3. Data transmission: All images I and the corresponding data are transmitted to the medical workstation 7. Thus, all information required for navigation is present on the workstation 7.

2.4. If desired or necessary, the imaging steps 2.2. and 2.3. can be repeated for  
10 other orientations of the C-arm of the X-ray device 1.

### 3. Navigation during the intervention:

During the intervention, the position-tracked catheter 5 or guidewire can be navigated without the need for further X-ray images:

3.1. Position measurement: First, the position of the patient 4 and of the  
15 catheter 5 is measured using the position measurement system 6.

3.2. Data gathering: Simultaneously, the ECG phase is measured using the ECG system 8.

3.3. Image selection: Based on the ECG phase, the corresponding image or the corresponding images from the image database obtained in 2.2. are selected by the  
20 workstation 7.

3.4. Graphic superposition: From the available data together with the position of the X-ray device 1, a virtual graphic superposition of the catheter on the selected X-ray image is carried out during the taking of the images, without further images having to be taken by X-ray.

25 3.5. Repetition: Steps 3.1.-3.4. are carried out continuously.

The arrangement as shown in the figure thus allows very precise intravascular or intracardial navigation on X-ray fluoroscopy images with a reduced amount of X-radiation.

According to a variant of the method, the latter can be carried out with a  
30 reduced update frequency. In this case, a reference image is selected from the multimodal data generated in step 2.2. For example, this may be the image from the end systolic phase of the cardiac cycle. Instead of again and again displaying images corresponding to the current ECG phase in steps 3.3. and 3.4., only the aforesaid reference image is used. That is to say that an update of the catheter position in step 3.4. on the reference image is only carried out

when the currently measured heartbeat phase corresponds to the heartbeat phase of the reference image (that is to say to the end systolic phase). In this way, the update rate is reduced to one update per cardiac cycle.

According to another development of the method, in step 2.2.2. additionally a  
5 breathing sensor is used, in order to measure the current breathing phase of the patient 4. The breathing phase is then stored along with the images I and the ECG phase in the multimodal data. In step 3.2., the breathing phase is likewise measured. In step 3.3., the associated image is then selected on the basis both of the ECG phase and of the breathing phase. The rest of the method then proceeds unchanged. If in phase 2.2. of data gathering not enough data can be  
10 obtained, then suitable interpolation methods can be used in order to calculate the superposed catheter position of the image. Furthermore, a movement correction for the breathing movement can be carried out as a result of the fact that the breathing-induced movement of the heart can be compensated for based on the measured breathing position using a movement model of the heart.

15 Another development of the method comprises mixing the steps of data gathering (2.2.-2.4.) and navigation (3.1.-3.5.) with one another. In this way, it is possible for the fundamental 2D images of the image database to be verified, in whole or in part, in real-time during the intervention, so that the image database that is used can be regularly refreshed in whole or in part.

## CLAIMS:

1. A method of tracking an instrument (5) that is inserted into the body of a patient (4), comprising the steps of:
  - a) detection of a movement signal which represents the movement phases of a periodic internal movement of the body;
  - 5 b) generation of 2D images (I) of a body volume of interest, and storage thereof in an image database together with the associated imaging parameters and the associated movement phase;
  - c) measurement of the spatial position of the instrument (5) and optionally of the spatial position of at least one reference probe (2, 3);
  - 10 d) selection of at least one 2D image from the image database, which 2D image corresponds in terms of its associated movement phase to the movement phase belonging to the measured spatial position of the instrument (5);
  - e) determination of the position of the instrument on the selected 2D image.
- 15 2. A method as claimed in claim 1, characterized in that an electrocardiogram and/or a breathing movement signal that is dependent on the breathing movement of the patient (4) is detected as movement signal.
3. A method as claimed in claim 1, characterized in that the position of the  
20 instrument (5) is represented superposed on the selected 2D images.
4. A method as claimed in claim 1, characterized in that, in step d), only 2D images from a single movement phase are available for selection from the image database.
- 25 5. A method as claimed in claim 1, characterized in that steps b) and c) to e) are carried out a number of times and in varying order.
6. A method as claimed in claim 1, characterized in that the image database contains 2D images from various projection directions.

7. A method as claimed in claim 1, characterized in that the 2D images are generated in step b) by means of X-radiation and/or ultrasound.

5 8. A method as claimed in claim 1, characterized in that at least one reference probe (2) is fitted on a movable X-ray device (1) which is provided for generating the 2D images (I).

9. A method as claimed in claim 1, characterized in that at least one reference  
10 probe (3) is arranged on or in the body of the patient.

10. A method as claimed in claim 1, characterized in that the breathing movement is compensated for using movement models of the body.

15 11. An arrangement for tracking an instrument (5) that is inserted into the body of a patient (4), comprising:

- a) a device (1) for generating 2D images (I) of a body volume of interest;
- b) a unit (6) for determining the set imaging parameters of the device (1);
- c) a signal measurement unit (8) for detecting a movement signal which  
20 represents the movement phases of a periodic internal movement of the body;
- d) a storage unit (7) for storing an image database of 2D images of the body volume together with the associated imaging parameters and the associated movement phases;
- e) a position measurement unit (6) for determining the spatial position of the  
25 instrument (5) that is inserted into the body and optionally the spatial position of at least one reference probe (2, 3);
- d) a control and computation unit (7) for selecting at least one 2D image from the image database, which 2D image corresponds in terms of its associated movement phase to the movement phase belonging to the spatial position of the instrument, and for  
30 determining the position of the instrument (5) on the selected 2D image.

12. An arrangement as claimed in claim 11, characterized in that it is designed for carrying out a method as claimed in at least one of claims 1 to 10.

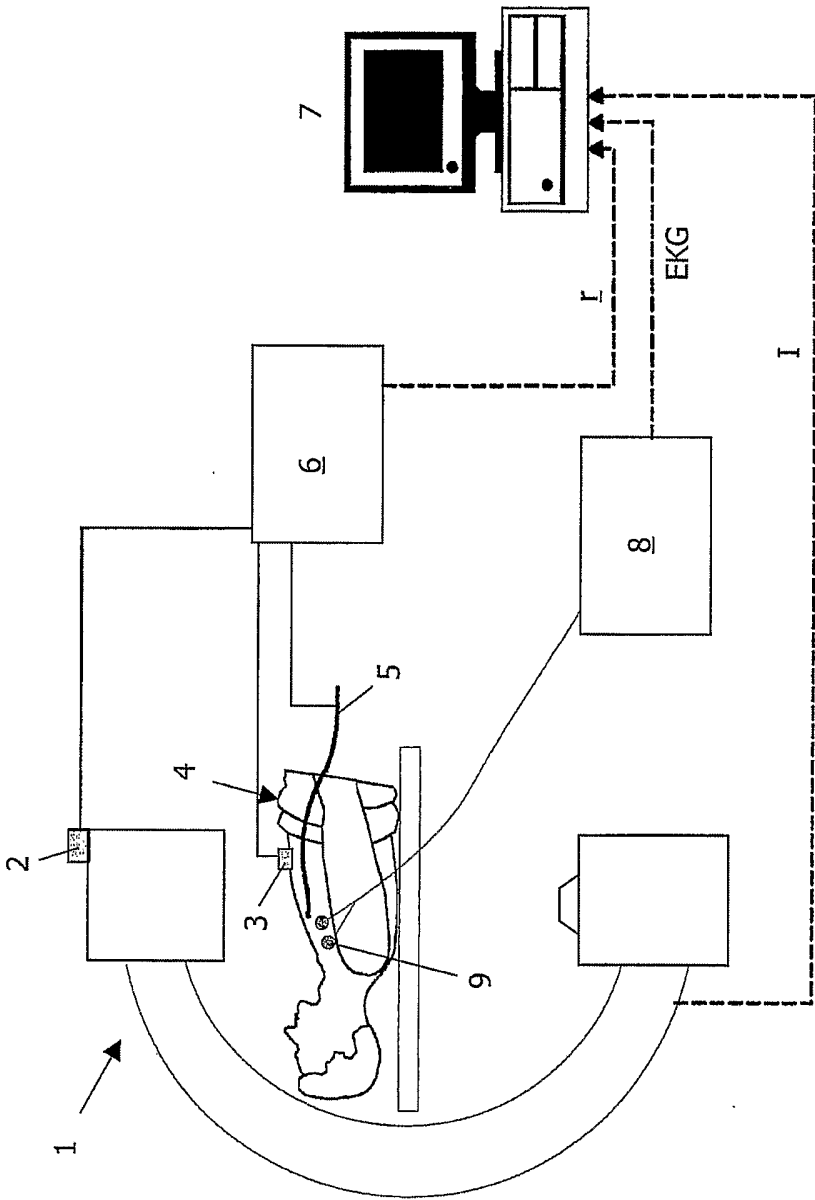


Fig. 1

# INTERNATIONAL SEARCH REPORT

Interr      Application No  
PCT/ID 03/06233

**A. CLASSIFICATION OF SUBJECT MATTER**  
IPC 7      A61B5/06      A61B6/12

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)  
IPC 7      A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)  
EPO-Internal

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2001/031919 A1 (EICHER UZI ET AL) 18 October 2001 (2001-10-18)	1-9, 11, 12
Y	paragraph '0018! - paragraph '0021! paragraph '0043! - paragraph '0045! paragraph '0047! - paragraph '0048! paragraph '0054! - paragraph '0055! paragraph '0067! - paragraph '0072! paragraph '0075! paragraph '0106! - paragraph '0110! paragraph '0115! - paragraph '0116! paragraph '0151! - paragraph '0159! claims 1-4, 8-14, 21-26, 28, 29, 31, 37-39, 101-105, 110, 114-119 figures 1, 6, 12  ---  -/--	10

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

\* Special categories of cited documents:

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- \*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
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Date of the actual completion of the international search

12 March 2004

Date of mailing of the international search report

19/03/2004

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,  
Fax: (+31-70) 340-3016

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 Intern: | Application No  
 PCT/IB 03/06233

## C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	WO 99 43253 A (BIOSENSE INC) 2 September 1999 (1999-09-02) page 5, line 16 -page 7, line 6 page 9, line 15 -page 9, line 18 page 10, line 3 -page 10, line 12 page 13, line 5 -page 13, line 21 page 15, line 19 -page 15, line 25 page 17, line 3 -page 18, line 14 claims 1,6,7,13-16 figure 1 ----	1-12
Y	WO 00 10456 A (SUPER DIMENSION LTD ;BLECHER DANNY (IL); GILBOA PINHAS (IL)) 2 March 2000 (2000-03-02) page 6, line 10 -page 6, line 16 page 11, line 1 -page 11, line 31 page 27, line 28 -page 29, line 31 figure 9 ----	1-12
Y	US 5 577 502 A (DARROW ROBERT D ET AL) 26 November 1996 (1996-11-26) column 3, line 28 -column 3, line 38 column 4, line 38 -column 4, line 55 column 6, line 22 -column 6, line 60 claims 1-3 figure 1 ----	1-12
Y	US 6 473 635 B1 (RASCHKE VOLKER) 29 October 2002 (2002-10-29) * whole document * ----	1-12
Y	US 5 265 610 A (DARROW ROBERT D ET AL) 30 November 1993 (1993-11-30) column 3, line 9 -column 3, line 32 column 7, line 49 -column 8, line 2 claims 1,13-17 figure 1 ----	1-12
Y	YI WANG ET AL: "Respiratory motion of the heart: kinematics and the implications for the spatial resolution in coronary imaging" MAGNETIC RESONANCE IN MEDICINE, ACADEMIC PRESS, DULUTH, MN, US, vol. 33, no. 5, May 1995 (1995-05), pages 713-719, XP002260907 ISSN: 0740-3194 * whole document * -----	10

# INTERNATIONAL SEARCH REPORT

Information on patent family members

Intern: Application No

PCT, 1.0 03/06233

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2001031919 A1	18-10-2001	US 6233476 B1 CA 2438089 A1 EP 1367941 A2 WO 02064011 A2 US 2002049375 A1 AU 4607600 A CA 2373295 A1 EP 1185199 A1 WO 0069335 A1 JP 2003520062 T	15-05-2001 22-08-2002 10-12-2003 22-08-2002 25-04-2002 05-12-2000 23-11-2000 13-03-2002 23-11-2000 02-07-2003
WO 9943253 A	02-09-1999	US 6580938 B1 AU 8281998 A CA 2287220 A1 EP 0977510 A1 JP 2001524863 T WO 9943253 A1	17-06-2003 15-09-1999 02-09-1999 09-02-2000 04-12-2001 02-09-1999
WO 0010456 A	02-03-2000	AU 4644799 A EP 1100373 A1 WO 0010456 A1 JP 2003524443 T US 2003160721 A1 US 2003216639 A1 US 6593884 B1 US 2001047133 A1 US 2002005719 A1 US 2002042571 A1	14-03-2000 23-05-2001 02-03-2000 19-08-2003 28-08-2003 20-11-2003 15-07-2003 29-11-2001 17-01-2002 11-04-2002
US 5577502 A	26-11-1996	US 5671739 A	30-09-1997
US 6473635 B1	29-10-2002	DE 19946948 A1 EP 1088514 A1 JP 2001170027 A	05-04-2001 04-04-2001 26-06-2001
US 5265610 A	30-11-1993	NONE	