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- (71) Applicant: **LIFESCAN SCOTLAND LIMITED**  
[GB/GB]; Beechwood Park North, Inverness IV2 3ED (GB).
- (72) Inventors: **WHITEHEAD, Neil**; Beechwood Park North, Inverness IV2 3ED (GB). **PHILLIPS, Stuart**; Beechwood Park North, Inverness IV2 3ED (GB). **MORRIS, David**; Beechwood Park North, Inverness IV2 3ED (GB). **MCILRATH, Ramsay**; Beechwood Park North, Inverness IV2 3ED (GB). **MACLEOD, Robert**; Beechwood Park North, Inverness IV2 3ED (GB). **WHYTE, Lynsey**; Beechwood Park North, Inverness IV2 3ED (GB). **CAMPBELL, Karn**; Beechwood Park North, Inverness IV2 3ED

(GB). **DARLING, Ramsay**; Beechwood Park North, Inverness IV2 3ED (GB). **MCLAREN, James**; Beechwood Park North, Inverness IV2 3ED (GB). **BAIN, Russell**; Beechwood Park North, Inverness IV2 3ED (GB).

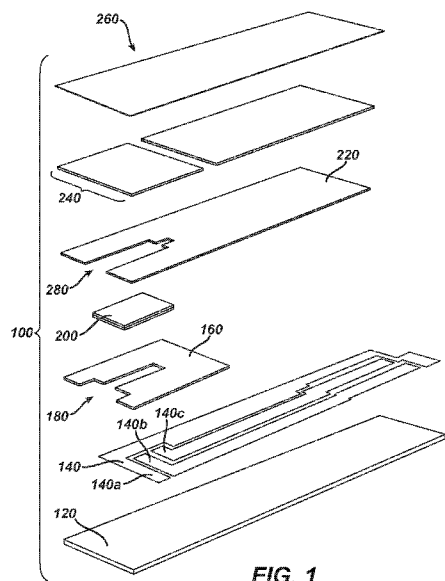
(74) Agents: **BRUNNER, John Michael Owen** et al.; Carpmaels & Ransford, One Southampton Row, London WC1B 5HA (GB).

(81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY, BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IS, JP, KE, KG, KM, KN, KP, KR, KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

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(54) Title: ELECTROCHEMICAL-BASED ANALYTICAL TEST STRIP WITH FILL-SPEED CONFIGURED REAGENT LAYER



(57) Abstract: An electrochemical-based analytical test strip ("EBAT") for the determination of an analyte in a bodily fluid sample includes an electrically insulating substrate layer with a distal end and a patterned conductor layer that is disposed over the electrically-insulating substrate layer and has a working electrode ("WE") and a counter/reference electrode ("C/RE"). The EBAT also includes a patterned insulation layer with an electrode exposure window configured to expose a WE exposed portion and a C/RE exposed portion, an enzymatic reagent layer; and a patterned spacer layer. In addition, the patterned insulation layer and the patterned spacer layer define a sample receiving chamber with a sample-receiving opening at the distal end of the electrically insulating substrate layer and that extends across the WE exposed portion and the C/RE exposed portion. Furthermore, the enzymatic reagent layer is disposed over the working electrode and counter/reference electrode exposed portions and extends no more than 400µm toward the sample-receiving opening.

WO 2013/117924 A1

EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, **Published:**  
LV, MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK, — *with international search report (Art. 21(3))*  
SM, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ,  
GW, ML, MR, NE, SN, TD, TG).

## **ELECTROCHEMICAL-BASED ANALYTICAL TEST STRIP WITH FILL-SPEED CONFIGURED REAGENT LAYER**

### **BACKGROUND OF THE INVENTION**

**[0001]** Field of the Invention

**[0002]** The present invention relates, in general, to medical devices and, in particular, to analytical test strips and related methods.

**[0003]** Description of Related Art

**[0004]** The determination (e.g., detection and/or concentration measurement) of an analyte in a fluid sample is of particular interest in the medical field. For example, it can be desirable to determine glucose, ketone bodies, cholesterol, lipoproteins, triglycerides, acetaminophen and/or HbA1c concentrations in a sample of a bodily fluid such as urine, blood, plasma or interstitial fluid. Such determinations can be achieved using analytical test strips, based on, for example, visual, photometric or electrochemical techniques. Conventional electrochemical-based analytical test strips are described in, for example, U.S. Patent Nos. 5,708,247, and 6,284,125, each of which is hereby incorporated in full by reference.

### **BRIEF DESCRIPTION OF THE DRAWINGS**

**[0005]** The accompanying drawings, which are incorporated herein and constitute part of this specification, illustrate presently preferred embodiments of the invention, and, together with the general description given above and the detailed description given below, serve to explain features of the invention, in which:

FIG. 1 is a simplified exploded view of an electrochemical-based analytical test strip according to an embodiment of the present invention;

FIG. 2 is a simplified semi-exploded view of the electrochemical-based analytical test strip of FIG. 1;

FIG. 3 is a simplified bottom outline view of a distal end portion of an electrically insulating substrate layer, patterned conductor layer, patterned insulating layer, reagent layer, patterned spacer layer, and hydrophilic layer of the electrochemical-based analytical test strip of FIG. 1;

FIG. 4 is a simplified top outline view of the patterned spacer layer, and hydrophilic layer of the electrochemical-based analytical test strip of FIG. 1;

FIGs. 5A-5C are simplified top views of the patterned spacer layer, hydrophilic layer and top layer of the electrochemical-based analytical test strip of FIG. 1; and

FIG. 5D is a simplified outline view of the layers of FIGs. 5A-5C integrated into a single component (i.e., an engineered top tape) prior to assembly of an electrochemical-based analytical test strip according to the present invention;

FIG. 6 is a graph of fill speed (i.e., "timing" in milliseconds) versus enzyme extension for an electrochemical-based analytical test strip according to an embodiment of the present invention; and

FIG. 7 is a flow diagram depicting stages in a method for determining an analyte in a bodily fluid sample according to an embodiment of the present invention.

## **DETAILED DESCRIPTION OF ILLUSTRATIVE EMBODIMENTS**

[0006] The following detailed description should be read with reference to the drawings, in which like elements in different drawings are identically numbered. The drawings, which are not necessarily to scale, depict exemplary embodiments for the purpose of explanation only and are not intended to limit the scope of the invention. The detailed description illustrates by way of example, not by way of limitation, the principles of the invention. This description will clearly enable one skilled in the art to make and use the invention, and describes several embodiments, adaptations, variations, alternatives and uses of the

invention, including what is presently believed to be the best mode of carrying out the invention.

[0007] As used herein, the terms “about” or “approximately” for any numerical values or ranges indicate a suitable dimensional tolerance that allows the part or collection of components to function for its intended purpose as described herein

[0008] In general, electrochemical-based analytical test strips for the determination of an analyte (such as glucose) in a bodily fluid sample (for example, whole blood) according to embodiments of the present invention include an electrically insulating substrate layer with a distal end and a patterned conductor layer that is disposed over the electrically-insulating substrate layer and has a working electrode and a counter/reference electrode. The electrochemical-based analytical test strips also include a patterned insulation layer with an electrode exposure window configured to expose a working electrode exposed portion and a counter/reference electrode exposed portion, a reagent layer, and a patterned spacer layer. In addition, the patterned insulation layer and the patterned spacer layer define a sample receiving chamber with a sample-receiving opening at the distal end of the electrically insulating substrate layer and that extends across the working electrode exposed portion and the counter/reference electrode exposed portion. Moreover, the reagent layer is disposed over the working electrode exposed portion and the counter/reference electrode exposed portion and extends no more than 400 $\mu$ m toward the sample-receiving opening beyond the distal most of the working electrode exposed portion and the counter/reference electrode exposed portion.

[0009] Electrochemical-based analytical test strips according to embodiments of the present invention are beneficial in that, for example, the fill speed of the electrochemical-based analytical test strip (e.g., the time for a bodily fluid sample to travel from one point to another point in a same-receiving chamber of the electrochemical-based analytical test strip (in this case it is the time taken for

fluid to travel between a first working electrode and a second working electrode. The start and end times of the speed measurement are triggered by an increase in current beyond a pre-determined threshold – in this case the threshold current is 150nA) and fill speed variability are beneficially optimized. Reduction in fill speed reduces the risk of generating a fill speed-related error message during analyte determination (the error risk is related to the accuracy check performed by the meter on the end currents of the first and second working electrodes. If a strip fills too slowly, the end currents of the first and second working electrodes may be sufficiently different to cause an Error 5 message i.e. >20% difference in end current after 5 seconds) and also reduces the delay experienced by a user in receiving determination results. A reduction in fill speed variability reduces a user's perception of strip-to-strip variation that can cause concern or annoyance.

[0010] FIG. 1 is a simplified exploded view of an electrochemical-based analytical test strip according to an embodiment of the present invention. FIG. 2 is a simplified semi-exploded view of the electrochemical-based analytical test strip of FIG. 1. FIG. 3 is a simplified bottom outline view of a distal portion of an electrically insulating substrate layer, patterned conductor layer, patterned insulating layer, reagent layer, patterned spacer layer, and hydrophilic layer of the electrochemical-based analytical test strip of FIG. 1. FIG. 4 is a simplified top outline view of the patterned spacer layer, and hydrophilic layer of the electrochemical-based analytical test strip of FIG. 1. FIGs. 5A-5C are simplified top views of the patterned spacer layer, hydrophilic layer and top layer of the electrochemical-based analytical test strip of FIG. 1. FIG. 5D is a simplified outline view of the layers of FIGs. 5A-5C integrated into a single component (i.e., an engineered top tape) prior to assembly of an electrochemical-based analytical test strip according to the present invention. FIG. 6 is a graph of fill speed (i.e., "timing" in milliseconds) versus enzyme extension for an electrochemical-based analytical test strip according to an embodiment of the present invention.

[0011] Referring to FIGs. 1-6, electrochemical-based analytical test strip 100 for the determination of an analyte (such as glucose) in a bodily fluid sample (for example, a whole blood sample) includes an electrically-insulating substrate layer 120, a patterned conductor layer 140, a patterned insulation layer 160 with electrode exposure window 180 therein, an enzymatic reagent layer 200, a patterned spacer layer 220, a hydrophilic layer 240, and a top layer 260.

[0012] The disposition and alignment of electrically-insulating substrate layer 120, patterned conductor layer 140 (which includes a counter/reference electrode 140a, a first working electrode 140b and a second working electrode 140c, see FIGs. 1 and 3 in particular), patterned insulation layer 160, enzymatic reagent layer 200, patterned spacer layer 220, hydrophilic layer 240 and top layer 260 of electrochemical-based analytical test strip 100 are such that sample-receiving chamber 280 is formed within electrochemical-based analytical test strip 100.

[0013] Although, for the purpose of explanation only, electrochemical-based analytical test strip 100 is depicted as including three electrodes, embodiments of electrochemical-based analytical test strips, including embodiments of the present invention, can include any suitable number of electrodes.

[0014] Counter/reference electrode 140a, first working electrode 140b, and second working electrode 140c can be formed of any suitable material including, for example, gold, palladium, platinum, indium, titanium-palladium alloys and electrically conducting carbon-based materials. Referring in particular to FIG. 3, electrode exposure window 180 of patterned insulation layer 160 exposes a portion of counter/reference electrode 140a, a portion of first working electrode 140b and a portion of second working electrode 140c (such portions being specked in FIG. 3). During use, a bodily fluid sample is applied to electrochemical-based analytical test strip 100 and transferred to sample-receiving chamber 280, thereby operatively contacting the

counter/reference electrode, first working electrode and second working electrode exposed portions.

**[0015]** Electrically-insulating substrate layer 120 can be any suitable electrically-insulating substrate layer known to one skilled in the art including, for example, a nylon substrate, polycarbonate substrate, a polyimide substrate, a polyvinyl chloride substrate, a polyethylene substrate, a polypropylene substrate, a glycolated polyester (PETG) substrate, or a polyester substrate. The electrically-insulating substrate layer can have any suitable dimensions including, for example, a width dimension of about 5 mm, a length dimension of about 27 mm and a thickness dimension of about 0.5 mm.

**[0016]** Electrically-insulating substrate layer 120 provides structure to the strip for ease of handling and also serves as a base for the application (e.g., printing or deposition) of subsequent layers (e.g., a patterned conductor layer). It should be noted that patterned conductor layers employed in analytical test strips according to embodiments of the present invention can take any suitable shape and be formed of any suitable materials including, for example, metal materials and conductive carbon materials.

**[0017]** Patterned insulation layer 160 can be formed, for example, from a screen printable insulating ink. Such a screen printable insulating ink is commercially available from Ercon of Wareham, Massachusetts U.S.A. under the name "Insulayer."

**[0018]** Patterned spacer layer 220 can be formed, for example, from a screen-printable pressure sensitive adhesive commercially available from Apollo Adhesives, Tamworth, Staffordshire, UK. In the embodiment of FIGs. 1 through 5C, patterned spacer layer 220 defines outer walls of the sample-receiving chamber 280.



**[0019]** Hydrophilic layer 240 can be, for example, a clear film with hydrophilic properties that promote wetting and filling of electrochemical-based analytical test strip 100 by a fluid sample (e.g., a whole blood sample). Such clear films are commercially available from, for example, 3M of Minneapolis, Minnesota U.S.A. If desired, patterned spacer layer 220, hydrophilic layer 240 and top layer 260 can be integrated into a single component 260' as depicted in FIG. 5D. Such an integrated component is also referred to as an Engineered Top Tape (ETT) and can be, for example, a pre-constructed laminate that defines the sides and top of the sample-receiving chamber. Suitable hydrophilic layers are commercially available from, for example, Coveme (San Lazzaro di Savena, Italy)

**[0020]** Enzymatic reagent layer 200 can include any suitable enzymatic reagents, with the selection of enzymatic reagents being dependent on the analyte to be determined. For example, if glucose is to be determined in a blood sample, enzymatic reagent layer 200 can include a glucose oxidase or glucose dehydrogenase along with other components necessary for functional operation. Enzymatic reagent layer 200 can include, for example, glucose oxidase, tri-sodium citrate, citric acid, polyvinyl alcohol, hydroxyl ethyl cellulose, potassium ferrocyanide, antifoam, cabosil, PVPVA, and water. Further details regarding enzymatic reagent layers, and electrochemical-based analytical test strips in general, are in U.S. Patent Nos. 6,241,862 and 6,733,655, the contents of which are hereby fully incorporated by reference.

**[0021]** Referring to FIG. 3 in particular, enzymatic reagent layer 200 is disposed over the first and second working electrode exposed portions and the counter/reference electrode exposed portion and extends no more than 400 $\mu$ m toward the distal end of the sample-receiving opening beyond the distal most of the working electrode exposed portion and the counter/reference electrode exposed portion. In other words, the enzymatic reagent layer extends no more than 400 $\mu$ m upstream of the distal most electrode. This distance is demarcated by the arrow labeled "A" in FIG. 3. As described above and illustrated by the data

of FIG. 6, limiting the extension of the enzymatic reagent layer to  $\leq 400\mu\text{m}$  provides an unexpectedly slow fill speed and an unexpectedly low fill variability.

[0022] FIG. 6 is a graph of fill speed (i.e., “timing” in milliseconds) versus enzyme extension for an electrochemical-based analytical test strip according to an embodiment of the present invention. The data of FIG. 6 was collected using whole blood bodily fluid samples and an electrochemical-based analytical test strip with a sample-receiving chamber volume of 0.73 micro-liters, a sample-receiving chamber height of 0.130mm, a sample-receiving chamber length of 3.77mm and a primary sample-receiving chamber width of 1.50mm.

[0023] Referring to FIG. 6, it is evident that extensions of no more than  $400\mu\text{m}$  and, in particularly, extensions in the range of  $200\mu\text{m}$  to  $400\mu\text{m}$  are unexpectedly beneficial with respect to optimizing (i.e., reducing) fill speed and fill speed variability.

[0024] It has been determined that electrochemical-based analytical test strips according to embodiments of the present invention are particularly beneficial with respect to optimizing fill speed and fill variability when the enzymatic reagent layer is relatively hydrophilic and/or has a chalky texture (i.e., has a powdery texture) prior to application of a bodily fluid sample to the electrochemical-based analytical test strip. It is hypothesized without being bound that chalky enzymatic reagent layers exhibit poor adhesion to the electrically-insulating substrate layer at a microscopic level that interferes with bodily fluid flow. Enzymatic reagent layers that contain silica can be relatively hydrophilic and/or have a chalky texture. Therefore, electrochemical-based analytical test strips according to embodiments of the present invention are also particularly beneficial when the enzymatic reagent layer contains silica.

[0025] Electrochemical-based analytical test strip 100 can be manufactured, for example, by the sequential aligned formation of patterned conductor layer 140, patterned insulation layer 160, enzymatic reagent layer 200, patterned spacer

layer 220, hydrophilic layer 240 and top layer 260 onto electrically-insulating substrate layer 120. Any suitable techniques known to one skilled in the art can be used to accomplish such sequential aligned formation, including, for example, screen printing, photolithography, photogravure, chemical vapour deposition and tape lamination techniques.

[0026] FIG. 7 is a flow diagram depicting stages in a method 600 for determining an analyte (such as glucose) in a bodily fluid sample according to an embodiment of the present invention. At step 610 of method 600, a bodily fluid sample is applied to an electrochemical-based analytical test strip such that the applied bodily fluid sample fills a sample-receiving chamber of the electrochemical-based analytical test strip. The electrochemical-based analytical test strip employed in step 610 has an electrically insulating substrate layer with a distal end and also has a patterned conductor layer (with a working electrode and a counter/reference electrode) that is disposed over the electrically-insulating layer. The electrochemical-based analytical test strip also has a patterned insulation layer with an electrode exposure window configured to expose a working electrode exposed portion and a counter/reference electrode exposed portion, an enzymatic reagent layer; and a patterned spacer layer. In addition, the patterned insulation layer and the patterned spacer layer define a sample receiving chamber with a sample-receiving opening at the distal end of the electrically insulating base layer and that extends across the working electrode exposed portion and the counter/reference electrode exposed portion. Moreover, the enzymatic reagent layer is disposed over the working electrode exposed portion and the counter/reference electrode exposed portion and extends no more than 400 $\mu$ m toward the sample-receiving opening beyond the distal most of the working electrode exposed portion and the counter/reference electrode exposed portion. In other words, the enzymatic reagent layer extends no more than 400 $\mu$ m upstream of the electrodes of the electrochemical-based analytical test strip as previously discussed with respect to FIG. 3.

[0027] Method 600 also includes measuring an electrochemical response of the electrochemical-based analytical test strip (see step 620 of FIG. 7) and, at step 630, determining the analyte based on the measured electrochemical response. The measuring and determination steps (i.e., steps 620 and 630) can, if desired, be performed using a suitable associated meter.

[0028] Once apprised of the present disclosure, one skilled in the art will recognize that method 600 can be readily modified to incorporate any of the techniques, benefits and characteristics of electrochemical-based analytical test strips according to embodiments of the present invention and described herein.

[0029] While preferred embodiments of the present invention have been shown and described herein, it will be obvious to those skilled in the art that such embodiments are provided by way of example only. Numerous variations, changes, and substitutions will now occur to those skilled in the art without departing from the invention. It should be understood that various alternatives to the embodiments of the invention described herein may be employed in practicing the invention. It is intended that the following claims define the scope of the invention and that devices and methods within the scope of these claims and their equivalents be covered thereby.

## CLAIMS

### WHAT IS CLAIMED IS:

1. An electrochemical-based analytical test strip for the determination of an analyte in a bodily fluid sample, the electrochemical-based analytical test strip comprising:

an electrically insulating substrate layer with a distal end;

a patterned conductor layer disposed over the electrically-insulating substrate layer, the patterned conductive layer including at least a working electrode and a counter/reference electrode;

a patterned insulation layer with an electrode exposure window configured to expose a working electrode exposed portion and a counter/reference electrode exposed portion

an enzymatic reagent layer; and

a patterned spacer layer,

wherein the patterned insulation layer and the patterned spacer layer define a sample receiving chamber with a sample-receiving opening at the distal end of the electrically insulating substrate layer and that extends across the working electrode exposed portion and the counter/reference electrode exposed portion, and

wherein the enzymatic reagent layer is disposed over the working electrode exposed portion and the counter/reference electrode exposed portion and extends no more than 400 $\mu$ m toward the sample-receiving opening beyond the distal most of the working electrode exposed portion and the counter/reference electrode exposed portion.

2. The electrochemical-based analytical test strip of claim 1 wherein the patterned spacer layer is formed of a hydrophilic material.

3. The electrochemical-based analytical test strip of claim 1 wherein the enzymatic reagent layer extends a distance in the range of 200 $\mu$ m to 400 $\mu$ m.

4. The electrochemical-based analytical test strip of claim 1 wherein the patterned conductor layer includes a first working electrode, a second working electrode and a counter/reference electrode.

5. The electrochemical-based analytical test strip of claim 1 wherein the analyte is glucose and the bodily fluid sample is blood.

6. The electrochemical-based analytical test strip of claim 1 wherein the enzymatic reagent layer has a chalky texture.

7. The electrochemical-based analytical test strip of claim 1 wherein the enzymatic reagent layer contains silica.

8. The electrochemical-based analytical test strip of claim 7 wherein the enzymatic reagent layer has a chalky texture.

9. The electrochemical-based analytical test strip of claim 1 further including:

a hydrophilic layer; and  
a top layer.

10. The electrochemical-based analytical test strip of claim 9 wherein the patterned spacer layer, hydrophilic layer and top layer are integrated into a single component.

11. A method for determining an analyte in a bodily fluid sample, the method comprising:

applying a bodily fluid sample to an electrochemical-based analytical test strip such that the applied bodily fluid sample fills a sample-receiving chamber of the electrochemical-based analytical test strip, the electrochemical-based analytical test

strip having:

an electrically insulating substrate layer with a distal end;

a patterned conductor layer disposed over the

electrically-insulating substrate layer, the patterned conductive layer including at least a working electrode and a counter/reference electrode;

a patterned insulation layer with an electrode exposure window configured to expose a working electrode exposed portion and a counter/reference electrode exposed portion;

an enzymatic reagent layer; and

a patterned spacer layer,

wherein the patterned insulation layer and the patterned spacer layer define the sample receiving chamber with a sample-receiving opening at the distal end of the electrically insulating substrate layer and that extends across the working electrode exposed portion and the counter/reference electrode exposed portion, and

wherein the reagent layer is disposed over the working electrode exposed portion and the counter/reference electrode exposed portion and extends no more than 400 $\mu$ m toward the sample-receiving opening beyond the distal most of the working electrode exposed portion and the counter/reference electrode exposed portion;

measuring an electrochemical response of the electrochemical-based analytical test strip; and

determining the analyte based on the measured electrochemical response.

12. The method of claim 11 wherein the bodily fluid sample is whole blood.

13. The method of claim 11 wherein the analyte is glucose.

14. The method of claim 11 wherein the patterned spacer layer is formed of a hydrophilic material.

15. The method of claim 11 wherein the enzymatic reagent layer extends a

distance in the range of 200 $\mu$ m to 400 $\mu$ m.

16. The method of claim 11 wherein the patterned conductor layer includes a first working electrode, a second working electrode and a counter/reference electrode.

17. The method of claim 11 wherein the enzymatic reagent layer has a chalky texture.

18. The method of claim 11 wherein the enzymatic reagent layer contains silica.

19. The method of claim 18 wherein the enzymatic reagent layer has a chalky texture.

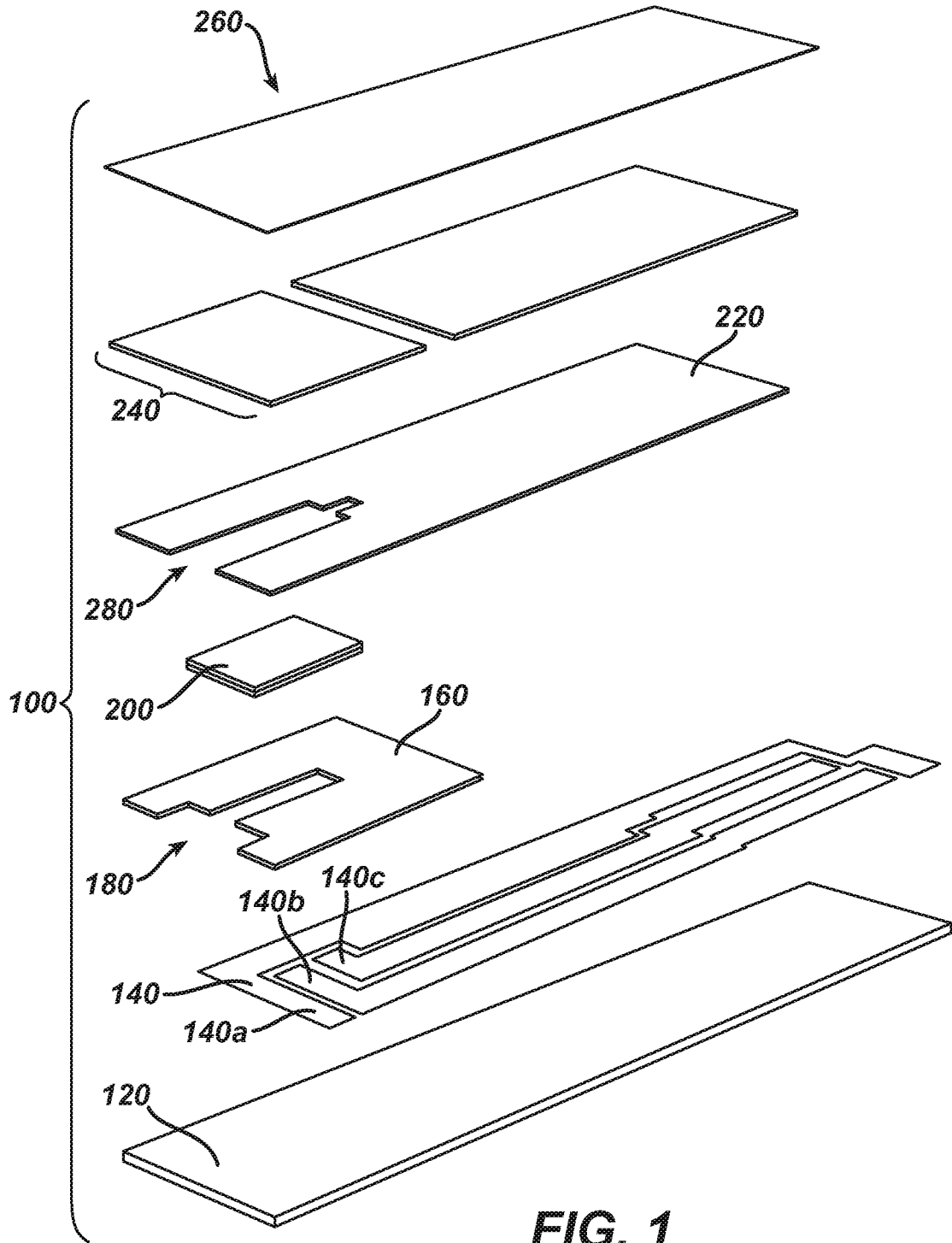
20. The method of claim 11 wherein the electrochemical-based analytical test strip further includes:

a hydrophilic layer; and  
a top layer.

21. The method of claim 20 wherein the patterned spacer layer, hydrophilic layer and top layer are integrated into a single component.

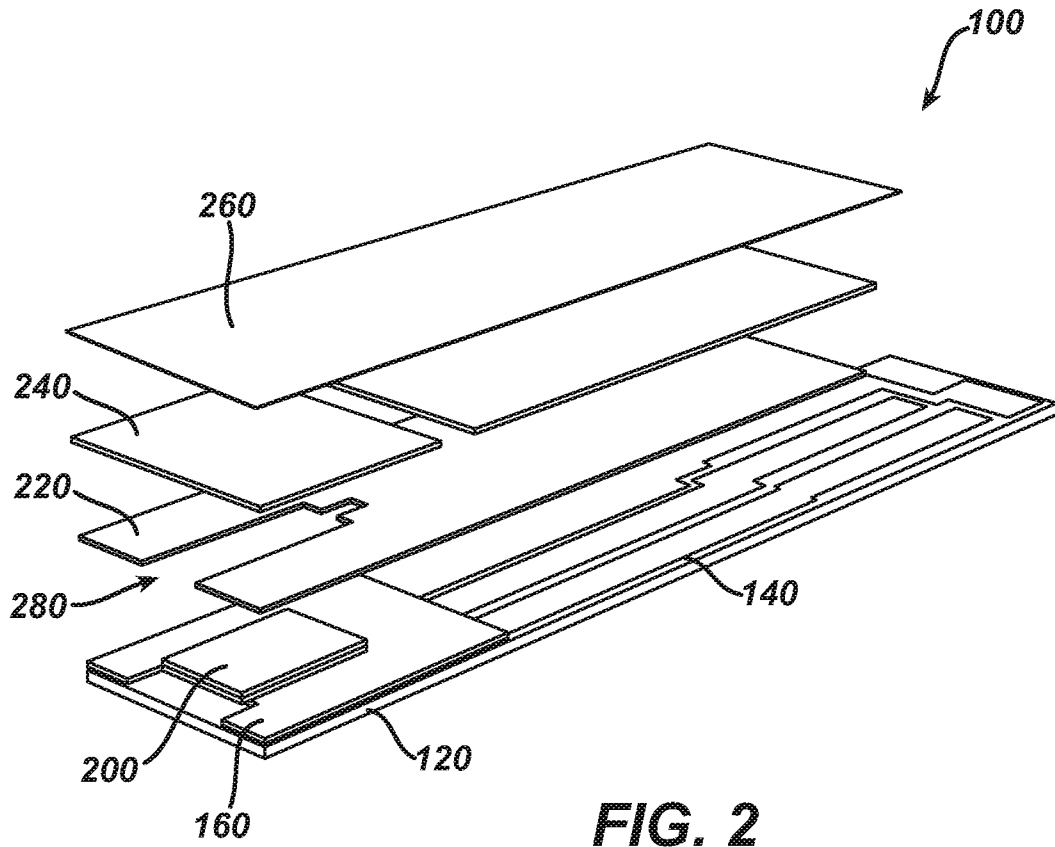


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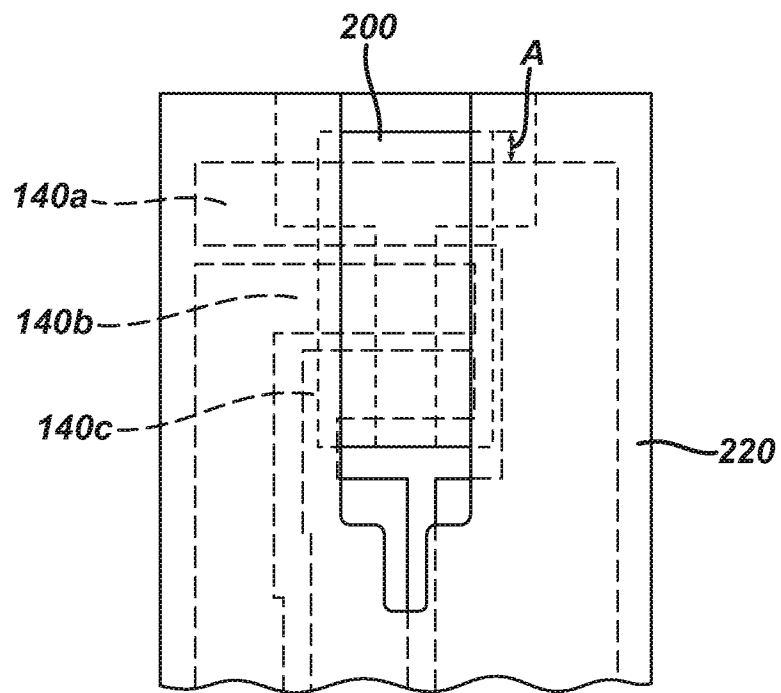
**FIG. 1**

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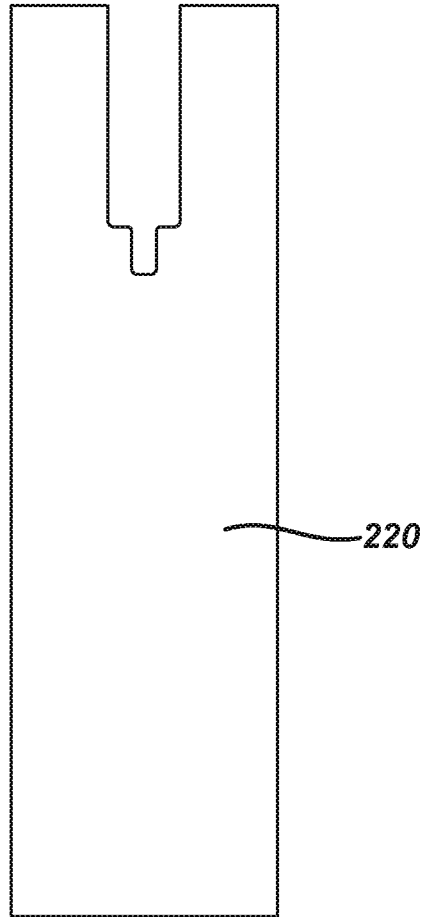
**FIG. 2**

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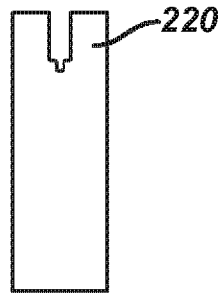


**FIG. 3**

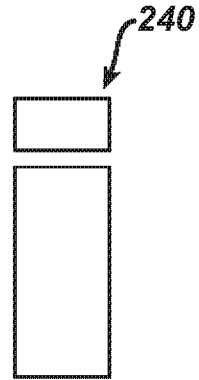
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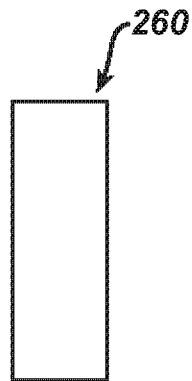
**FIG. 4**



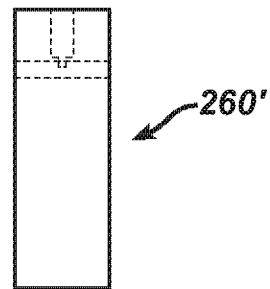
**FIG. 5A**



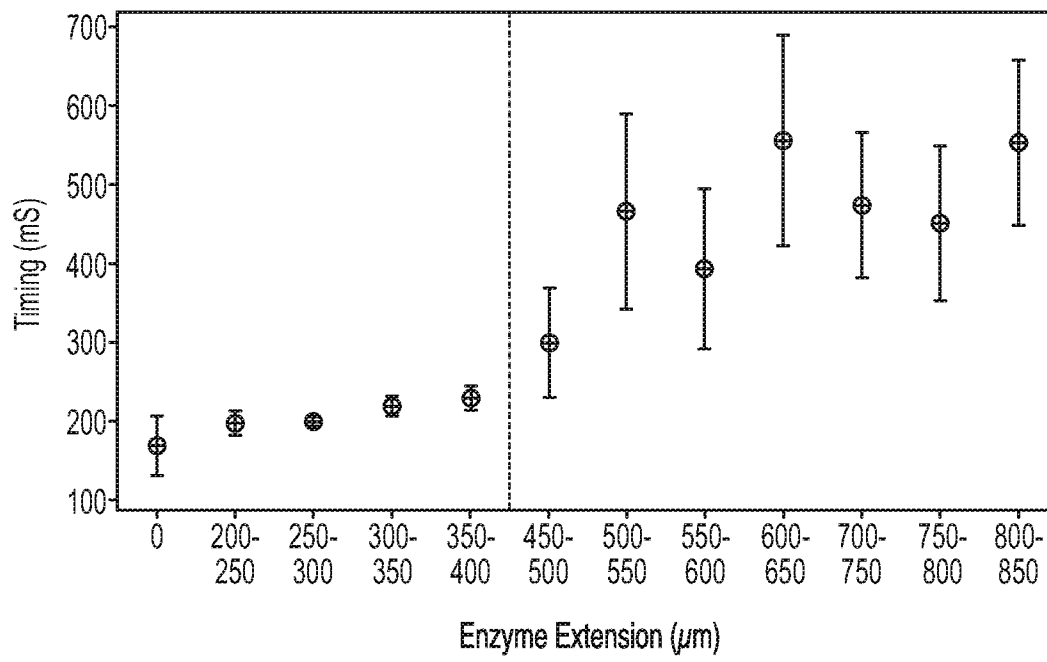
**FIG. 5B**



**FIG. 5C**

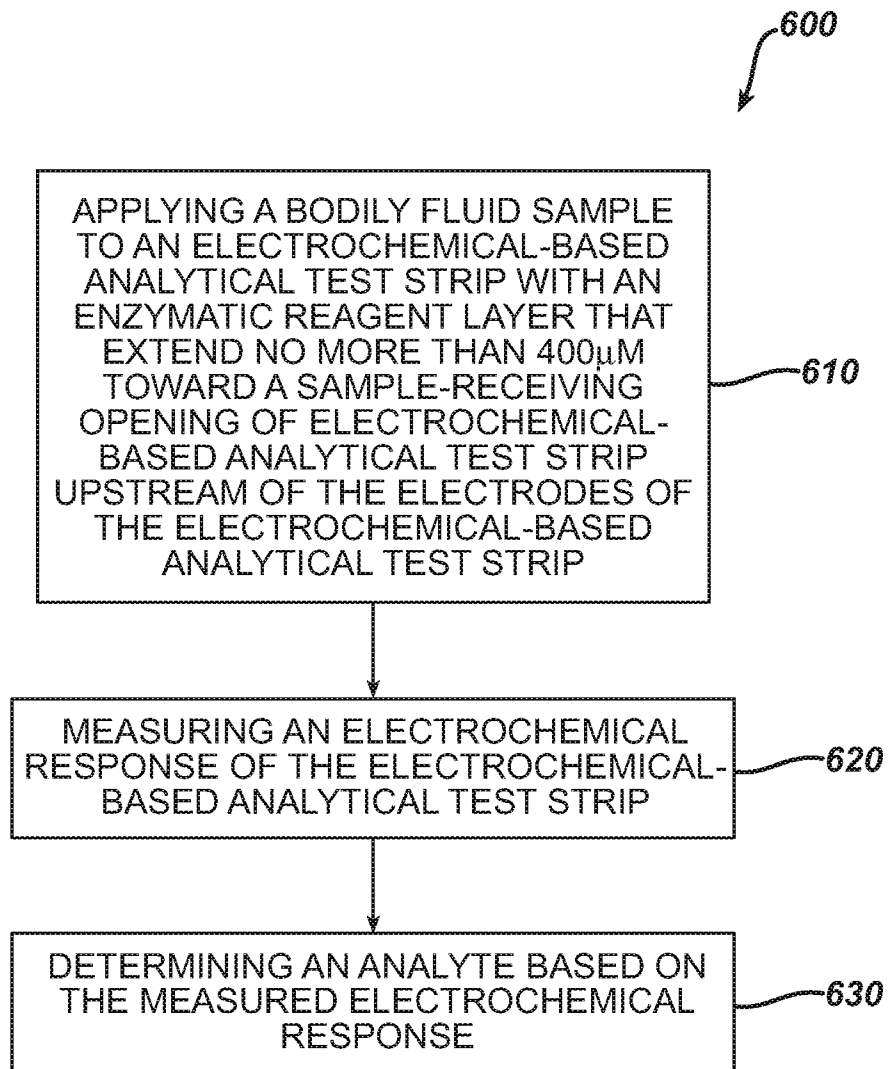


**FIG. 5D**



**FIG. 6**

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**FIG. 7**

INTERNATIONAL SEARCH REPORT

International application No  
PCT/GB2013/050275

A. CLASSIFICATION OF SUBJECT MATTER  
INV. C12Q1/00  
ADD.  
  
According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED  
Minimum documentation searched (classification system followed by classification symbols)  
C12Q  
  
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)  
EPO-Internal, BIOSIS, EMBASE, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	EP 2 182 355 A2 (LIFESCAN SCOTLAND LTD [GB]) 5 May 2010 (2010-05-05) the whole document	1-21
A	WO 2004/093784 A2 (HOME DIAGNOSTICS INC [US]; NEEL GARY T [US]; BELL DOUGLAS E [US]; WONG) 4 November 2004 (2004-11-04) p.12, lines 14-24; fig.2-3; claim 1	1-21
A	GB 2 391 945 A (E2V TECH UK LTD [GB] E2V TECH UK LTD [GB]; E2V TECH [GB]) 18 February 2004 (2004-02-18) claims 1, 27	1-21

Further documents are listed in the continuation of Box C.

See patent family annex.

\* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
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Date of the actual completion of the international search

17 April 2013

Date of mailing of the international search report

10/05/2013

Name and mailing address of the ISA/

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Fax: (+31-70) 340-3016

Authorized officer

Pellegrini, Paolo



**INTERNATIONAL SEARCH REPORT**

Information on patent family members

International application No

PCT/GB2013/050275

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