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(54) **AUGMENTATION OU REPARATION D'ANOMALIES DES  
TISSUS CUTANES, SOUS-CUTANES OU DES CORDES  
VOCALES**

(54) **AUGMENTATION AND REPAIR OF DERMAL,  
SUBCUTANEOUS, AND VOCAL CORD TISSUE DEFECTS**

(57) La présente invention concerne une méthodologie d'augmentation à long terme et/ou de réparation de tissus cutanés, sous-cutanés ou des cordes vocales, par injection ou implantation chirurgicale directe de fibroblastes cultivés autologues provenant d'un tissu conjonctif, ou dermique, ou aponévrotique, ou de fibroblastes provenant de tissus du chorion de l'intestin ou d'adipocytes. Les fibroblastes cultivés utilisés pour l'augmentation et/ou la réparation d'anomalies cutanées proviennent d'un tissu conjonctif, et/ou dermique et/ou aponévrotique. L'invention concerne en outre une méthodologie qui permet de cultiver des cellules sensiblement débarrassées des protéines potentiellement immunogènes contenues dans le sérum en faisant passer, au stade final de leur culture, les fibroblastes issus de tissus du chorion de l'intestin ou d'adipocytes dans un milieu exempt de sérum, ou encore dans le propre sérum du patient.

(57) This invention is a methodology for the long-term augmentation, and/or repair of dermal, subcutaneous, or vocal cord tissue by the injection, or direct surgical placement of autologous cultured fibroblasts derived from connective tissue, or dermis, or fascia lamina propria tissue fibroblasts derived from the lamina propria or adipocytes. The fibroblast cultures utilized for the augmentation, and/or repair of skin defects are derived from either connective tissue, dermal, and/or fascial fibroblasts. In addition a methodology of rendering the cultured cells substantially free of potentially immunogenic serum derived proteins by late stage passage of the cultured fibroblasts lamina propria tissue, or adipocytes in serum free medium in the patient's own serum.

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## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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<b>(21) International Application Number:</b> PCT/US98/03439 <b>(22) International Filing Date:</b> 20 February 1998 (20.02.98) <b>(30) Priority Data:</b> 60/037,961                      20 February 1997 (20.02.97)      US 09/003,328                      6 January 1998 (06.01.98)        US <b>(71) Applicant (for all designated States except US):</b> GERIGENE MEDICAL CORPORATION [US/US]; 565 Science Drive, Madison, WI 53711 (US). <b>(72) Inventor; and</b> <b>(75) Inventor/Applicant (for US only):</b> KLEINSEK, Don, A. [-/US]; W5036 NCTHA, Elkhart Lake, WI 53020 (US). <b>(74) Agent:</b> SCANLON, William, J.; Scanlon Law Office, 616 S. Ingersoll Street, Madison, WI 53703 (US).	<b>(81) Designated States:</b> AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, GH, GM, GW, HU, ID, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, UA, UG, US, UZ, VN, YU, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).  <b>Published</b> <i>With international search report.</i> <i>Before the expiration of the time limit for amending the</i> <i>claims and to be republished in the event of the receipt of</i> <i>amendments.</i>	
<b>(54) Title:</b> AUGMENTATION AND REPAIR OF DERMAL, SUBCUTANEOUS, AND VOCAL CORD TISSUE DEFECTS		
<b>(57) Abstract</b>  This invention is a methodology for the long-term augmentation, and/or repair of dermal, subcutaneous, or vocal cord tissue by the injection, or direct surgical placement of autologous cultured fibroblasts derived from connective tissue, or dermis, or fascia lamina propria tissue fibroblasts derived from the lamina propria or adipocytes. The fibroblast cultures utilized for the augmentation, and/or repair of skin defects are derived from either connective tissue, dermal, and/or fascial fibroblasts. In addition a methodology of rendering the cultured cells substantially free of potentially immunogenic serum derived proteins by late stage passage of the cultured fibroblasts lamina propria tissue, or adipocytes in serum free medium in the patient's own serum.		

AUGMENTATION AND REPAIR OF DERMAL, SUBCUTANEOUS,  
AND VOCAL CORD TISSUE DEFECTS

5 FIELD OF INVENTION

The field of the present invention is the long-term augmentation and/or repair of defects in dermal, subcutaneous, or vocal cord tissue.

BACKGROUND OF THE INVENTION

10 I. IN VITRO CELL CULTURE

The majority of in vitro vertebrate cell cultures are grown as monolayers on an artificial substrate which is continuously bathed in a nutrient medium. The nature of the substrate on which the monolayers may be grown may be either a solid (e.g., plastic) or a semi-solid (e.g., collagen or  
15 agar). Currently, disposable plastics have become a preferred substrate for cell culture.

While the growth of cells in two-dimensions is frequently used for the preparation and examination of cultured cells *in vitro*, it lacks the characteristics of intact, *in vivo* tissue which, for example, includes cell-cell  
20 and cell-matrix interactions. Therefore, in order to characterize these functional and morphological interactions, various investigators have examined the use of three-dimensional substrates in such forms as a collagen gel (Yang *et al.*, *Cancer Res.* 41:1027 (1981); Douglas *et al.*, *In Vitro* 16:306 (1980); Yang *et al.*, *Proc. Nat'l Acad. Sci.* 2088 (1980) ), cellulose sponge  
25 (Leighton *et al.*, *J. Nat'l Cancer Inst.* 12:545 (1951) ), collagen-coated cellulose sponge (Leighton *et al.*, *Cancer Res.* 28:286 (1968) ), and GELFOAM® (Sorour *et al.*, *J. Neurosurq.* 43:742 (1975) ). Typically, these aforementioned three-dimensional substrates are inoculated with the cells to be cultured, which subsequently penetrate the substrate and establish a

"tissue-like" histology similar to that found *in vivo*. Several attempts to regenerate "tissue-like" histology from dispersed monolayers of cells utilizing three-dimensional substrates have been reported. For example, three-dimensional collagen substrates have been utilized to culture a variety of cells including breast epithelium (Yang, *Cancer Res.* 41:1021 (1981)), vascular epithelium (Folkman *et al.*, *Nature* 288 :551 (1980)), and hepatocytes (Sirica *et al.*, *Cancer Res.* 76:3259 (1980)). However, long-term culture and proliferation of cells in such systems has not yet been achieved. Prior to the present invention, a three-dimensional substrate had not been utilized in the autologous *in vitro* culture of cells or tissues derived from the dermis, fascia, or lamina propria.

## II. AUGMENTATION AND/OR REPAIR OF DERMAL AND SUBCUTANEOUS TISSUES

In the practice of cosmetic and reconstructive plastic surgery, it is frequently necessary to employ the use of various injectable materials to augment and/or repair defects of the subcutaneous or dermal tissue, thus effecting an aesthetic result. Non-biological injectable materials (*e.g.*, paraffin) were first utilized to correct facial contour defects as early as the late nineteenth century. However, numerous complications and the generally unsatisfactory nature of long-term aesthetic results caused the procedure to be rapidly abandoned. More recently, the use of injectable silicone became prevalent in the 1960's for the correction of minor defects, although various inherent complications also limited the use of this substance. Complications associated with the utilization of injectable liquid silicone include local and systemic inflammatory reactions, formation of scar tissue around the silicone droplets, rampant and frequently distant, unpredictable migration throughout

the body, and localized tissue breakdown. Due to these potential complications, silicone is not currently approved for general clinical use. Although the original proponents of silicone injection have continued experimental programs utilizing specially manufactured "Medical Grade" silicone (*e.g.*, Dow Corning's MDX 4.4011®) with a limited number of subjects, it appears highly unlikely that its use will be generally adopted by the surgical community. See *e.g.*, Spira and Rosen, *Clin. Plastic Surgery* 20:181 (1993); Matton *et al.*, *Aesthetic Plastic Surgery* 9:133 (1985).

It has also been suggested to compound extremely small particulate species in a lubricious material and inject such micro-particulate media subcutaneously for both soft and hard tissue augmentation and repair. However, success has been heretofore limited. For example, bioreactive materials such as hydroxyapatite or coral granules (osteo conductive) have been utilized for the repair of hard tissue defects. Subsequent undesirable micro-particulate media migration and serious granulomatous reactions frequently occur with the injection of this material. These undesirable effects are well-documented with the use of such materials as polytetrafluoroethylene (TEFLON®) spheres of small-diameter (~ 90% of particles having diameters of  $\leq 30\mu\text{m}$ ) in glycerin. See *e.g.*, Malizia *et al.*, *JAMA* 251:3277 (1984). Additionally, the use of very small-diameter particulate spheres (~1-20 $\mu\text{m}$ ) or small elongated fibrils (~1-30 $\mu\text{m}$  in diameter) of various materials in a biocompatible fluid lubricant as injectable implant composition are disclosed in U.S. Patent No. 4,803,075. However, while these aforementioned materials create immediate augmentation and/or repair of defects, they also have a tendency to migrate and be reabsorbed from the original injection site.

The poor results initially obtained with the use of non-biological injectable materials prompted the use of various non-immunogenic, proteinaceous materials (e.g., bovine collagen and fibrin matrices). Prior to human injection, however, the carboxyl- and amino-terminal peptides of bovine collagen must first be enzymatically degraded, due to its highly immunogenic nature. Enzymatic degradation of bovine collagen yields a material, atelocollagen, which can be used in limited quantities in patients pre-screened to exclude those who are immunoreactive to this substance. The methodologies involved in the preparation and clinical utilization of atelocollagen are disclosed in U.S. Patent Nos. 3,949,073; 4,424,208; and 4,488,911. Atelocollagen has been marketed as ZYDERM® brand atelocollagen solution in concentrations of 35 mg/ml and 65 mg/ml. Although atelocollagen has been widely employed, the use of ZYDERM solution has been associated with the development of antibovine antibodies in approximately 90% of patients and with overt immunological complications in 1-3% of patients. See DeLustro *et al.*, *Plastic and Reconstructive Surgery* 79:581 (1987).

Injectable atelocollagen solution also was shown to be absorbed from the injection site, without replacement by host material, within a period of weeks to months. Clinical protocols calling for repeated injections of atelocollagen are, in practice, primarily limited by the development of immunogenic reactions to the bovine collagen. In order to mitigate these limitations, bovine atelocollagen was further processed by cross-linking with 0.25% glutaraldehyde, followed by filtration and mechanical shearing through fine mesh. The methodologies involved in the preparation and clinical utilization of this material are disclosed in U.S. Patent Nos. 4,582,640 and 4,642,117. The modified atelocollagen was marketed as

ZYPLAST® brand cross-linked bovine atelocollagen. The properties and advantages of cross-linking were to provide increased resistance to host degradation, however this was offset by an increase in solution viscosity. In addition, cross-linking of the bovine atelocollagen was found to decrease the number of host cells which infiltrated the injected collagen site. The increased viscosity, and in particular irregular increased viscosity resulting in "lumpiness," not only rendered the material more difficult to utilize, but also made it unsuitable for use in certain circumstances. See e.g., U.S. Patent No. 5,366,498. In addition, several investigators have reported that there is no or marginally-increased resistance to host degradation of ZYPLAST cross-linked bovine atelocollagen in comparison to that of the non-cross-linked ZYDERM atelocollagen solution and that the overall longevity of the injected material is, at best, only 4-6 months. See e.g., Ozgentas et al., *Ann. Plastic Surgery* 33:171 (1994); and Matti and Nicolle, *Aesthetic Plastic Surgery* 14:227 (1990).

Moreover, bovine atelocollagen cross-linked with glutaraldehyde may retain this agent as a high molecular weight polymer which is continuously hydrolyzed, thus facilitating the release of monomeric glutaraldehyde. The monomeric form of glutaraldehyde is detectable in body tissues for up to 6 weeks after the initial injection of the cross-linked atelocollagen. The cytotoxic effect of glutaraldehyde on in vitro fibroblast cultures is indicative of this substance's not being an ideal cross-linking agent for a dermal equivalent which is eventually infiltrated host cells and in which the bovine atelocollagen matrix is rapidly degraded, thus resulting in the release of monomeric glutaraldehyde into the bodily tissues and fluids. Similarly, chondroitin-6-sulfate (GAG), which weakly binds to collagen at neutral pH, has also been utilized to chemically modify bovine protein for

tissue graft implantation. See Hansborough and Boyce, JAMA 136:2125 (1989). However, like glutaraldehyde, GAG may be released into the tissue causing unforeseen long-term effects on human subjects. GAG has been reported to increase scar tissue formation in wounds, which is to be avoided in grafts. Additionally, a reduction of collagen blood clotting capacity may also be deleterious in the application in bleeding wounds, as fibrin clot contributes to an adhesion of the graft to the surrounding tissue.

The limitations which are imposed by the immunogenicity of both modified and non-modified bovine atelocollagen have resulted in the isolation of human collagen from placenta (see e.g., U.S. Patent No. 5,002,071); from surgical specimens (see e.g., U.S. Patent Nos. 4,969,912 and 5,332,802); and cadaver (see e.g., U.S. Patent No. 4,882,166). Moreover, processing of human-derived collagen by cross-linking and similar chemical modifications is also required, as human collagen is subject to analogous degradative processes as is bovine collagen. Human collagen for injection, derived from a sample of the patient's own tissue, is currently available and is marketed as AUTOLOGEN®. It should be noted, however, that there is no quantitative evidence which demonstrates that human collagen injection results in lower levels of implant degradation than that which is found with bovine collagen preparations. Furthermore, the utilization of autologous collagen preparation and injection is limited to those individuals who have previously undergone surgery, due to the fact that the initial culture from which the collagen is produced is derived from the tissue removed during the surgical procedure. Therefore, it is evident that, although human collagen circumvents the potential for immunogenicity exhibited by bovine collagen, it fails to provide long-term therapeutic benefits and is limited to those patients who have undergone prior surgical procedures.

An additional injectable material currently in use as an alternative to atelocollagen augmentation of the subjacent dermis consists of a mixture of gelatin powder,  $\epsilon$ -aminocaproic acid, and the patient's plasma marketed as FIBREL®. See Multicenter Clinical Trial, *J. Am. Acad. Dermatology* 5 16:1155 (1987). The action of the FIBREL product appears to be dependent upon the initial induction of a sclerogenic inflammatory response to the augmentation of the soft tissue via the subcutaneous injection of the material. See e.g., Gold, *J. Dermatologic Surg. Oncology*, 20:586 (1994). Clinical utilization of the FIBREL product has been reported to often result in an 10 overall lack of implant uniformity. (i.e., "lumpiness") and longevity, as well as complaints of patient discomfort associated with its injection. See e.g., Millikan et al., *J. Dermatologic. Surg. Oncology*, 17:223 (1991). Therefore, in conclusion, none of the currently utilized protein-based injectable materials appears to be totally satisfactory for the augmentation and/or repair of the 15 subjacent dermis and soft tissue.

The various complications associated with the utilization of the aforementioned materials have prompted experimentation with the implantation (grafting) of viable, living tissue to facilitate augmentation and/or repair of the subjacent dermis and soft tissue. For example, surgical 20 correction of various defects has been accomplished by initial removal and subsequent re-implantation of the excised adipose tissue either by injection (see e.g., Davies et al., *Arch. of Otolaryngology-Head and Neck Surgery* 121:95 (1995); McKinney & Pandya, *Aesthetic Plastic Surgery* 18:383 (1994); and Lewis, *Aesthetic Plastic Surgery*, 17:109 (1993)) or by the larger 25 scale surgical-implantation (see e.g., Ersck, *Plastic & Reconstructive Surgery* 87:219 (1991) ). To perform both of the aforementioned techniques a volume of adipose tissue equal or greater than is required for the subsequent

augmentation or repair procedure must be removed from the patient. Thus, for large scale repair procedures (e.g., breast reconstruction) the amount of adipose tissue which can be surgically-excised from the patient may be limiting. In addition, other frequently encountered difficulties with the  
5   aforementioned methodologies include non-uniformity of the injectate, unpredictable longevity of the aesthetic effects, and a 4-6 week period of post-injection inflammation and swelling. In contrast, in a preferred embodiment, the present invention utilizes the surgical engraftment of autologous adipocytes which have been cultured on a solid support typically  
10   derived from, but not limited to, collagen or isolated extracellular matrix. The culture may be established from a simple skin biopsy specimen and the amount of adipose tissue which can be subsequently cultured in vitro is not limited by the amount of adipose tissue initially excised from the patient.

Living skin equivalents have been examined as a methodology for  
15   the repair and/or replacement of human skin. Split thickness autographs' epidermal autographs (cultured autogenic keratinocytes), and epidermal allografts (cultured allogenic keratinocytes) have been used with a varying degree of success. However, unfortunately, these forms of treatment have all exhibited numerous disadvantages. For example, split thickness autographs  
20   generally show limited tissue expansion, require repeated surgical operations, and give rise to unfavorable aesthetic results. Epidermal autographs require long periods of time to be cultured, have a low success ("take") rate of approximately 30-48%, frequently form spontaneous blisters, exhibit contraction to 60-70% of their original size, are vulnerable during the  
25   first 15 days of engraftment, and are of no use in situations where there is both epidermal and dermal tissue involvement. Similarly, epidermal allografts (cultured allogenic keratinocytes) exhibit many of the limitations which are

inherent in the use of epidermal autographs. Additional methodologies have been examined which involve the utilization of irradiated cadaver dermis. However, this too has met with limited success due to, for example, graft rejection and unfavorable aesthetic results. Living skin equivalents

5 comprising a dermal layer of rodent fibroblast cells cast in soluble collagen and an epidermal layer of cultured rodent keratinocytes have been successfully grafted as allografts onto Sprague Dawley rats by Bell et al., J. Investigative Dermatology 81:2 (1983). Histological examination of the engrafted tissue revealed that the epidermal layer had fully differentiated to

10 form desmosomes, tonofilaments, keratohyalin, and a basement lamella. However, subsequent attempts to reproduce the living skin equivalent using human fibroblasts and keratinocytes has met with only limited success. In general, the keratinocytes failed to fully differentiate to form a basement lamella and the dermo-epidermal junction was a straight line.

15 The present invention includes the following methodologies for the repair and/or augmentation of various skin defects: (1) the injection of autologously cultured dermal or fascial fibroblasts into various layers of the skin or injection directly into a "pocket" created in the region to be repaired or augmented, or (2) the surgical engraftment of "strands" derived from

20 autologous dermal and fascial fibroblasts which are cultured in such a manner as to form a three-dimensional "tissue-like" structure similar to that which is found in vivo.

Moreover, the present invention also differs on a two-dimensional level in that "true" autologous culture and preparation of the cells is

25 performed by utilization of the patient's own cells and serum for in vi tro culture.

### III. VOCAL CORD TISSUE AUGMENTATION AND/OR REPAIR

Phonation is accomplished in humans by the passage of air past a pair of vocal cords located within the larynx. Striated muscle fibers within the larynx, comprising the constrictor muscles, function so as to vary the degree of tension in the vocal cords, thus regulating both their overall rigidity and proximity to one another to produce speech. However, when one (or both) of the vocal cords becomes totally or partially immobile, there is a diminution in the voice quality due to inability to regulate and maintain the requisite tension and proximity of the damaged cord in relation to that of the operable cord. Vocal cord paralysis may be caused by cancer, surgical or mechanical trauma, or similar afflictions which render the vocal cord incapable of being properly tensioned by the constrictor muscles.

One therapeutic approach which has been examined to allow phonation involves the implantation or injection of biocompatible materials. It has long been recognized that a paralyzed or damaged vocal cord may be repositioned or supported so as to remain in a fixed location relative to the operable cord such that the unilateral vibration of the operable cord produces an acceptable voice pattern. Hence, various surgical have been developed which involve the formation of the thyroid cartilage and subsequently providing a means for the support and/or repositioning of the paralyzed vocal cord.

For example, injection of TEFLON into the paralyzed vocal cord to increase its inherent "bulk" has been described. See e.g., von Leden et al., *Phonosurgery* 3:175 (1989). However, this procedure is now considered unacceptable due to the inability of the injected TEFLON to close large glottic gaps, as well as its tendency to induce inflammatory reactions resulting in the formation of fibrous infiltration into the injected cord. See

e.g., Maves et al., Phonosurgery: Indications and Pitfalls 98:577 (1989).

Moreover, removal of the injected TEFLON may be quite difficult should it subsequently be desired or become necessary.

Another methodology for supporting the paralyzed vocal cord  
5 which has been employed involves the utilization of a custom-fitted block of  
siliconized rubber (SILASTIC®). In order to ensure the proper fit of the  
implant, the surgeon hand carves SILASTIC block during the procedure in  
order to maximize the ability of the patient to phonate. The patient is kept  
under local anesthesia so that he or she can produce sounds to test the  
10 positioning of the implant. Generally, the implanted blocks are formed into  
the shape of a wedge which is totally implanted within the thyroid cartilage  
or a flanged plug which can be moved back-and-forth within the opening in  
the thyroid cartilage to fine-tune the voice of the patient.

Although SILASTIC implants have proved to be superior over  
15 TEFLON injections, there are several areas of dissatisfaction with the  
procedure including difficulty in the carving and insertion of the block, the  
large amount of time required for the procedure, and a lack of an efficient  
methodology for locking the block in place within the thyroid cartilage.  
In addition, vocal-cord edema, due to the prolonged nature of the procedure  
20 and repeated voice testing during the operation, may also prove problematic  
in obtaining optimal voice quality.

Other methodologies which have been utilized in the treatment of  
vocal cord paralysis and damage include GELFOAM® hydroxyapatite, and  
porous ceramic implants, as well as injections of silicone and collagen. See,  
25 e.g., Kaufman, Laryngoplastic Phonosurgery (1988). However, these  
materials have also proved to be less than ideal due to difficulties in the  
sizing and shaping of the solid implants as well as the potential for

subsequent immunogenic reactions. Therefore, there still remains a need for the development of a methodology which allows the efficacious treatment of vocal cord paralysis and/or damage.

## 5 SUMMARY OF THE INVENTION

The present invention discloses a methodology for the longterm augmentation and/or repair of dermal, subcutaneous, or vocal cord tissue by the injection or direct surgical placement/implantation of: (1) autologous cultured fibroblasts derived from connective tissue, dermis, or fascia; (2) lamina propria tissue; (3) fibroblasts derived from the lamina propria or (4) adipocytes. The fibroblast cultures utilized for the augmentation and/or repair of skin defects are derived from either connective tissue, dermal, and/or fascial fibroblasts. Typical defects of the skin which can be corrected with the injection or direct surgical placement of autologous fibroblasts or adipocytes include rhytids, stretch marks, depressed scars, cutaneous depressions of traumatic or non-traumatic origin, hypoplasia of the lip, and/or scarring from acne vulgaris. Typical defects of the vocal cord which can be corrected by the injection or direct surgical placement of lamina propria or autologous cultured fibroblasts from lamina propria include scarred, paralyzed, surgically or traumatically injured, or congenitally underdeveloped vocal cord(s).

The use of autologous cultured fibroblasts derived from the dermis, fascia, connective tissue, or lamina propria mitigates the possibility of an immunogenic reaction due to a lack of tissue histocompatibility. This provides vastly superior post-surgical results. In a preferred embodiment of the present invention, fibroblasts of connective tissue, dermal, or fascial origin as well as adipocytes are derived from full

biopsies of the skin. Similarly, lamina propria tissue or fibroblasts obtained from the lamina propria are obtained from vocal cord biopsies. It should be noted that the aforementioned from the individual who will subsequently undergo the surgical procedure, thus mitigating the potential for an immunogenic reaction. These tissues are then expanded in vitro utilizing standard tissue culture methodologies.

Additionally, the present invention further provides a methodology of rendering the cultured cells substantially free of potentially immunogenic serum-derived proteins by late-stage passage of the cultured fibroblasts, lamina propria tissue, or adipocytes in serum-free medium or in the patient's own serum. In addition, immunogenic proteins may be markedly reduced or eliminated by repeated washing in phosphate-buffered saline (PBS) or similar physiologically-compatible buffers.

## DESCRIPTION OF THE INVENTION

### I. HISTOLOGY OF THE SKIN

The skin is composed of two distinct layers: the epiderm a specialized epithelium derived from the ectoderm, and beneath this, the dermis, a vascular dense connective tissue, a derivative of mesoderm. These two layers are firmly adherent to one another and form a region which varies in overall thickness from approximately 0.5 to 4 mm in different areas of the body. Beneath the dermis is a layer of loose connective tissue which varies from areolar to adipose in character. This is the superficial fascia of gross anatomy, and is sometimes referred as the hypodermis, but is not considered to be part of the skin. The dermis is connected to the hypodermis by connective tissue fibers which pass from one layer to the other.

## A. EPIDERMIS

The epidermis, a stratified squamous epithelium, is composed of cells of two separate and distinct origins. The majority of the epithelium, of ectodermal origin, undergoes a process of keratinization resulting in the formation of the dead superficial layers of skin. The second component comprises the melanocytes which are involved in the synthesis of pigmentation via melanin. The latter cells do not undergo the process of keratinization. The superficial keratanized cells are continuously lost from the surface and must be replaced by cells that arise from the mitotic activity of cells of the basal layers of the epidermis. Cells which result from this proliferation are displaced to higher levels, and as they move upward they elaborate keratin, which eventually replaces the majority of the cytoplasm. As the process of keratinization continues the cell dies and is finally shed. Therefore, it should be appreciated that the structural organization of the epidermis into layers reflects various stages in the dynamic process of cellular proliferation and differentiation.

## B. DERMIS

It is frequently difficult to quantitatively differentiate the limits of the dermis as it merges into the underlying subcutaneous layer (hypodermis). The average thickness of the dermis varies from 0.5 to 3 mm and is further subdivided into two strata - the papillary layer superficially and the reticular layer beneath. The papillary layer is composed of thin collagenous, reticular, and elastic fibers arranged in an extensive network. Just beneath the epidermis, reticular fibers of the dermis form a close network into which the basal processes of the cells of the stratum germinativum are anchored. This region is referred to as the basal lamina.

The reticular layer is the main fibrous bed of the dermis. Generally, the papillary layer contains more cells and smaller and finer connective tissue fibers than the reticular layer. It consists of coarse, dense, and interlacing collagenous fibers, in which are intermingled a small number of reticular fibers and a large number of elastic fibers. The predominant arrangement of these fibers is parallel to the surface of the skin. The predominant cellular constituent of the dermis are fibroblasts and macrophages. In addition, adipose cells may be present either singly or, more frequently, in clusters. Owing to the direction of the fibers, lines of skin tension, Langer's lines, are formed. The overall direction of these lines is of surgical importance since incisions made parallel with the lines tend to gape less and heal with less scar tissue formation than incisions made at right-angles or obliquely across the lines. Pigmented, branched connective tissue cells, chromatophores, may also be present. These cells do not elaborate pigment but, instead, apparently obtain it from melanocytes.

Smooth muscle fibers may also be found in the dermis. These fibers are arranged in small bundles in connection with hair follicles (arrectores pilorum muscles) and are scattered throughout the dermis in considerable numbers in the skin of the nipple, penis, scrotum, and parts of the perineum. Contraction of the muscle fibers gives the skin of these regions a wrinkled appearance. In the face and neck, fibers of some skeletal muscles terminate in delicate elastic fiber networks of the dermis.

### C. ADIPOSE TISSUE/ADIPOCYTES

Fat cells, or adipocytes, are scattered in areolar connective tissue. When adipocytes form large aggregates, and are the principle cell type, the tissue is designated adipose tissue. Adipocytes are fully differentiated cells

and are thus incapable of undergoing mitotic division. New adipocytes therefore, which may develop at any time within the connective tissue, arise as a result of differentiation of more primitive cells. Although adipocytes, prior to the storage of lipid, resemble fibroblasts, it is likely that they arise  
5 directly from undifferentiated mesenchymal tissue.

Each adipocyte is surrounded by a web of fine reticular fibers; in the spaces between are found fibroblasts, lymphoid cells, eosinophils, and some mast cells. The closely spaced adipocytes form lobules, separated by fibrous septa. In addition, there is a rich network of capillaries in and between  
10 the lobules. The richness of the blood supply is indicative of the high rate of metabolic activity of adipose tissue.

It should be appreciated that adipose tissue is not static. There is a dynamic balance between lipid deposit and withdrawal. The lipid contained within adipocytes may be derived from three sources. Adipocytes, under the  
15 influence of the hormone insulin, can synthesize fat from carbohydrate. They can also produce fat from various fatty acids which are derived from the initial breakdown of dietary fat. Fatty acids may also be synthesized from glucose in the liver and transported to adipocytes as serum lipoproteins. Fats derived from different sources also differ chemically. Dietary fats may be  
20 saturated or unsaturated, depending upon the individual diet. Fat which is synthesized from carbohydrate is generally saturated. Withdrawals of fat result from enzymatic hydrolysis of stored fat to release fatty acids into the blood stream. However, if there is a continuous supply of exogenous glucose, then fat hydrolysis is negligible. The normal homeostatic balance is affected  
25 by hormones, principally insulin, and by the autonomic nervous system, which is responsible for the mobilization of fat from adipose tissue.

Adipose tissue may develop almost anywhere areolar tissue is prevalent, but in humans the most common sites of adipose tissue accumulation are the subcutaneous tissues (where it is referred to as the panniculus adiposus), in the mesenteries and omenta, in the bone marrow, and surrounding the kidneys. In addition to its primary function of storage and metabolism of neutral fat, in the subcutaneous tissue, adipose tissue also acts as a shock absorber and insulator to prevent excessive heat loss or gain through the skin.

## 10 II. HISTOLOGY OF THE LARYNX AND VOCAL CORDS

The larynx is that part of the respiratory system which connects the pharynx and trachea. In addition to its function as part of the respiratory system, it plays an important role in phonation (speech). The wall of the larynx is composed of a "skeleton" of hyaline and elastic cartilages, collagenous connective tissue, striated muscle, and mucous glands. The major cartilages of the larynx (the thyroid, cricoid, and arytenoids) are hyaline, whereas the smaller cartilages (the corniculates, cuneiforms, and the tips of the arytenoids) are elastic, as is the cartilage of the epiglottis. The aforementioned cartilages, together with the hyoid bone, are connected by three large, flat membranes: the thyrohyoid, the quadrates, and the cricovocal. These are composed of dense fibroconnective tissue in which many elastic fibers are present, particularly in the cricovocal membrane. The true and false vocal cords (vocal-and vestibular ligaments) are, respectively, the free upper borders of the cricovocal (cricothyroid) and the free lower borders of the quadrate (aryspiglottic) membranes. Extending laterally on each side between the true and false cords are the sinus and saccule of the larynx, a small slit-like diverticulum. Behind the cricoid and arytenoid

cartilages, the posterior wall of the pharynx is formed by the striated muscle of the pharyngeal constrictor muscles.

The epithelium of the mucous membrane of the larynx varies with location. For example, over the vocal folds, the lamina propria of the stratified squamous epithelium is extremely dense and firmly bound to the underlying connective tissue of the vocal ligament. While there is no true submucosa in the larynx, the lamina propria of the mucous membrane is thick and contains large numbers of elastic fibers.

### III. METHODOLOGIES

#### 10 A. IN VITRO CELL CULTURE OF FIBROBLASTS OR LAMINA PROPRIA

While the present invention may be practiced by utilizing any type of non-differentiated mesenchymal cell found in the skin which can be expanded in in vi tro culture, fibroblasts derived from dermal, connective tissue, fascial, lamina proprial tissue adipocytes, and/or extracellular tissues (matrix) derived from the cells are utilized in a preferred embodiment due to their relative of isolation and in vi tro expansion in tissue culture. In general, tissue culture techniques which are suitable for the propagation of non-differentiated mesenchymal cells may be used to expand the aforementioned cells/tissue and practice present invention as further discussed below. See e.g., Culture of Animal Cells: A Manual of Basic Techniques, Freshney, R. I., ed., (Alan R. Liss & Co., New York 1987); Animal Cell Culture: A Practical Approach, Freshney, R.I. ed., (IRL Press, Oxford, England (1986), whose references are incorporated herein by reference.

The utilization of autologous engraftment is a preferred therapeutic methodology due to the potential for graft rejection associated

with the use of allograft-based engraftment. Autologous grafts (i.e., those derived directly from the patient ensure histocompatibility by initially obtaining a tissue sample via biopsy directly from the patient who will be undergoing the corrective surgical procedure and then subsequently culturing fibroblasts derived from the dermal, connective tissue, fascial, or lamina proprial regions contained therein.

While the following sections will primarily discuss the autologous culture of fibroblasts of connective tissue, dermal, or fascial origins, in vitro culture of lamina propria tissue may also be established utilizing analogous methodologies. An autologous fibroblast culture is preferably initiated by the following methodology. A full-thickness biopsy of the skin (~3x6 mm) is initially obtained through, for example, a punch biopsy procedure. The specimen is repeatedly washed with antibiotic and anti-fungal agents prior to culture. Through a process of sterile microscopic dissection, the keratinized tissue-containing epidermis and subcutaneous adipocyte-containing tissue is removed, thus ensuring that the resultant culture is substantially free of non-fibroblast cells (e.g., adipocytes and keratinocytes). The isolated adipocytes-containing tissue may then be utilized to establish adipocyte cultures. Alternately, whole tissue may be cultured and fibroblast-specific growth medium may be utilized to "select" for these cells.

Two methodologies are generally utilized for the autologous culture of fibroblasts in the practice of the present invention - mechanical and enzymatic. In the mechanical methodology, the fascia, dermis, or connective tissue is initially dissected out and finely divided with scalpal or scissors. The finely minced pieces of the tissue are initially placed in 1-2 ml of medium in either a 5 mm petri dish (Costar), a 24 multi-well culture plate (Corning), or other appropriate tissue culture vessel.

Incubation is preferably performed at 37 deg. C in a 5% CO<sub>2</sub> atmosphere and the cells are incubated until a confluent monolayer of fibroblasts has been obtained. This may require up to 3 weeks of incubation. Following the establishment of confluence, the monolayer is trypsinized to  
5 release the adherent fibroblasts from the walls of the culture vessel. The suspended cells are collected by centrifugation, washed in phosphate-buffered saline, and resuspended in culture medium and placed into larger culture vessels containing the appropriate complete growth medium.

In a preferred embodiment of the enzymatic culture methodology,  
10 pieces of the finely minced tissue are digested with a protease for varying periods of time. The enzymatic concentration and incubation time are variable depending upon the individual tissue source, and the initial isolation of the fibroblasts from the tissue as well as the degree of subsequent outgrowth of the cultured cells are highly dependent upon these two factors. Effective  
15 proteases include, but are not limited to, trypsin, chymotrypsin, papain, chymopapain, and similar proteolytic enzymes. Preferably, the tissue is incubated with 200-1000 U/ml of collagenase type II for a time period ranging from 30 minutes to 24 hours, as collagenase type II was found to be highly efficacious in providing a high yield of viable fibroblasts. Following  
20 enzymatic digestion, the cells are collected by centrifugation and resuspended into fresh medium in culture flasks.

Various media may be used for the initial establishment of an in vitro culture of human fibroblasts. Dulbecco's Modified Eagle Medium (DMEM, Gibco/BRL Laboratories) with concentrations  
25 of fetal bovine serum (FBS), cosmic calf serum (CCS) or the patient's own serum varying from 5-20% (v/v) -- with higher concentrations resulting in faster culture growth -- are readily utilized for fibroblast culture. It should be

noted that substantial reductions in the concentration of serum (i.e., 0.5% v/v) results in a loss of cell viability in culture. In addition, the complete culture medium typically contains Lglutamine, sodium bicarbonate, pyridoxine hydrochloride, 1g/liter glucose, and gentamycin sulfate. The use  
5 of the patient's own serum mitigates the possibility of subsequent immunogenic reaction due to the presence of constituent antigenic proteins in the other serums.

Establishment of a fibroblast cell line from an initial human biopsy specimen generally requires 2 to 3.5 weeks in total. Once the initial culture  
10 has reached confluence, the cells may be passaged into new culture flasks following trypsinization by standard methodologies known within the relevant field. Preferably, for expansion, cultures are "split" 1:3 or 1:4 into T-150 culture flasks (Corning) yielding  $\sim 5 \times 10^7$  cells/culture vessel. The capacity of the T-150 culture flask is typically reached following 5-8 days of  
15 culture at which time the cultured cells are found to be confluent or near confluent.

Cells are preferably removed for freezing and long-term storage during the early passage stages of culture, rather than the later stages due to the fact that human fibroblasts are capable of undergoing a finite numbers of  
20 passages. Culture medium containing 70% DMEM growth medium, 10% (v/v) serum, and 20% (v/v) tissue culture grade dimethylsulfoxide (DMSO, Gibco/BRL) may be effectively utilized for freezing of fibroblast cultures. Frozen cells can subsequently be used to inoculate secondary cultures to obtain additional fibroblasts for use in the original patient, thus  
25 doing away with the requirement to obtain a second biopsy specimen. -

To minimize the possibility of subsequent immunogenic reactions in the engraftment patient, the removal of the various antigenic constituent

proteins contained within the serum may be facilitated by collection of the fibroblasts by centrifugation, washing the cells repeatedly in phosphate-buffered saline (PBS) and then either re-suspending or culturing the washed fibroblasts for a period of 2-24 hours in serum-free medium containing requisite growth factors which are well known in the field. Culture media include, but are not limited to, Fibroblast Basal Medium (FBM). Alternately, the fibroblasts may be cultured utilizing the patient's own serum in the appropriate growth medium.

After the culture has reached a state of confluence or sub-confluence, the fibroblasts may either be processed for injection or further cultured to facilitate the formation of a three-dimensional "tissue" for subsequent surgical engraftment. Fibroblasts utilized for injection consist of cells suspended in a collagen gel matrix or extracellular matrix. The collagen gel matrix is preferably comprised of a mixture of 2 ml of a collagen solution containing 0.5 to 1.5 mg/ml collagen in 0.05% acetic acid, 1 ml of DMEM medium, 270 µl of 7.5% sodium bicarbonate, 48 microliters of 100 micrograms/ml solution of gentamycin sulfate, and up to  $5 \times 10^6$  fibroblast cell/ml of collagen gel. Following the suspension of the fibroblasts in the collagen gel matrix, the suspension is allowed to solidify for approximately 15 minutes at room temperature or 37 deg C in a 5% CO<sub>2</sub> atmosphere. The collagen may be derived from human or bovine sources, or from the patient and may be enzymatically- or chemically-modified (e.g., atelocollagen).

Three-dimensional "tissue" is formed by initially suspending the fibroblasts in the collagen gel matrix as described above. Preferably, in the culture of three-dimensional tissue, full-length collagen is utilized, rather than truncated or modified collagen derivatives. The resulting suspension is then placed into a proprietary "transwell" culture system which is typically

comprised of culture well in which the lower growth medium is separated from the upper region of the culture well by a microporous membrane. The microporous membrane typically possesses a pore size ranging from 0.4 to 8  $\mu\text{m}$  in diameter and is constructed from materials including, but not limited to, polyester, nylon, nitrocellulose, cellulose acetate, polyacrylamide, cross-linked dextrose, agarose, or other similar materials. The culture well component of the transwell culture system may be fabricated in any desired shape or size (e.g., square, round, ellipsoidal, etc.) to facilitate subsequent surgical tissue engraftment and typically holds a volume of culture medium ranging from 200  $\mu\text{l}$  to 5 ml. In general, a concentration ranging from  $0.5 \times 10^6$  to  $10 \times 10^6$  cells/ml, and preferably  $5 \times 10^6$  cells/ml, are inoculated into the collagen/fibroblast-containing suspension as described above. Utilizing a preferred concentration of cells (i.e.,  $5 \times 10^6$  cells/ml), a total of approximately 4-5 weeks is required for the formation of a three-dimensional tissue matrix. However, this time may vary with increasing or decreasing concentrations of inoculated cells. Accordingly, the higher the concentration of cells utilized the less time due to a higher overall rate of cell proliferation and replacement of the exogenous collagen with endogenous collagen and other constituent materials which form the extracellular matrix synthesized by the cultured fibroblasts. Constituent materials which form the extracellular matrix include, but are not limited to, collagen, elastin, fibrin, fibrinogen, proteases, fibronectin, laminin, fibrellins, and other similar proteins. It should be noted that the potential for immunogenic reaction in the engrafted patient is markedly reduced due to the fact that the exogenous collagen used in establishing the initial collagen/fibroblast-containing suspension is gradually replaced during subsequent culture by endogenous collagen and extracellular matrix materials synthesized by the fibroblasts.

**B. IN VITRO CULTURE OF ADIPOCYTES**

Adipocytes require a "feeder-layer" or other type of solid support on which to grow. One potential solid support may be provided by utilization of the previously discussed collagen gel matrix. Alternately, the solid support  
5 may be provided by cultured extracellular matrix. In general, the *in vitro* culture of adipocytes is performed by the mechanical or enzymatic disaggregation of the adipocytes from adipose tissue derived from a biopsy specimen. The adipocytes are "seeded" onto the surface of the  
aforementioned solid support and allowed to grow until near-confluence is  
10 reached. The adipocytes are removed by gentle scraping of the solid surface. The isolated adipocytes are then cultured in the same manner as utilized for fibroblasts as previously discussed in Section III A.

**C. ISOLATION OF THE EXTRACELLULAR MATRIX**

15 The extracellular matrix (ECM) may be isolated in either a cellular or acellular form. Constituent materials which form the ECM include, but are not limited to, collagen, elastin, fibrin, fibrinogen, proteases, fibronectin, laminin, fibrellins, and other similar proteins. ECM is typically isolated by the initial culture of cells derived from skin, subcutaneous tissue, or vocal-  
20 cord biopsy specimens as previously described. After the cultured cells have reached a minimum of 25-50% sub-confluence, the ECM may be obtained by mechanical, enzymatic, chemical, or denaturant treatment. Mechanical collection is performed by scraping the ECM off of the plastic culture vessel and re-suspending in phosphate-buffered saline (PBS) . If desired, the  
25 constituent cells are lysed or ruptured by incubation in hypotonic saline containing 5 mM EDTA. Preferably, however, scraping followed by PBS re-suspension is generally utilized. Enzymatic treatment involves brief

incubation with a proteolytic enzyme such as trypsin. Additionally, the use of detergents such as sodium dodesyl sulfate (SDS) or treatment with denaturants such as urea or dithiotheritol (DTT) followed by dialysis against PBS, will also facilitate the release of the ECM from surrounding associated  
5 tissue.

The isolated ECM may then be utilized as a "filler" material in the various augmentation or repair procedures disclosed in the present application. In addition, the ECM may possess certain cell growth- or metabolism-promoting characteristics.

10

D. *IN VITRO* CULTURE OF FETAL OR JUVENILE CELLS CR  
TISSUES

In another preferred embodiment, rather than utilizing the patient's own tissue, all of the aforementioned cells, cell suspensions, or tissues may  
15 be derived from fetal or juvenile sources or sources that have been exposed to the sun little or not at all and, in any case, less than the tissue being repaired. Fetal cells lack the immunogenic determinants responsible for eliciting the host graft-rejection reaction and thus may be utilized for engraftment procedures with little or no probability of a subsequent  
20 immunogenic reaction. An acellular ECM may also be obtained from fetal ECM by hypotonic lysing of the constituent cells. The acellular ECM derived from fetal or juvenile or less sun-exposed sources or from *in vitro* culture of early passage cells typically possesses differs in both quantity and characteristics from that of the ECM derived from senescent or late-  
25 passage cells. The cellular or acellular ECM derived from fetal or juvenile sources may be used as a "filler" material in the various augmentation or repair procedures disclosed in the present application. In addition, the fetal

or juvenile ECM may possess certain cell growth- or metabolism-promoting characteristics.

E. INJECTION OF AUTOLOGOUS CULTURED  
5 DERMAL/FASCIAL FIBROBLASTS

To augment or repair dermal defects, autologously cultured fibroblasts are injected initially into the lower dermis, next in the upper and middle dermis, and finally in the subcutaneous regions of the skin as to form raised areas or "wheals." The fibroblast suspension is injected via a syringe  
10 with a needle ranging from 30 to 18 gauge, with the gauge of the needle being dependent upon such factors as the overall viscosity of the fibroblast suspension and the type of anesthetic utilized. Preferably, needles ranging from 22 to 18 gauge and 30 to 27 gauge are used with general and local anesthesia, respectively.

15 To inject the fibroblast suspension into the lower dermis, the needle is placed at approximately a 45° angle to the skin with the bevel of the needle directed downward. To place the fibroblast suspension into the middle dermis the needle is placed at approximately a 20-30° angle. To place the suspension into the upper dermis, the needle is placed almost horizontally  
20 (i.e., 10-15° angle). Subcutaneous injection is accomplished by initial placement of the needle into the subcutaneous tissue and injection of the fibroblast suspension during subsequent needle withdrawal. In addition, it should be noted that the needle is preferably inserted into the skin from various directions such that the needle tract will be somewhat different with  
25 each subsequent injection. This technique facilitates a greater amount of total skin area receiving the injected fibroblast suspension.

Following the aforementioned injections, the skin should be

expanded and possess a relatively taut feel. Care should be taken so as not to produce an overly hard feel to the injected region. Preferably, depressions or rhytids appear elevated following injection and should be "overcorrected" by a slight degree of over-injection of the fibroblast suspension, as typically  
5 some degree of settling or shrinkage will occur post-operatively.

In some scenarios, the injections may pass into deeper tissue layers. For example, in the case of lip augmentation or repair, a preferred manner of injection is accomplished by initially injecting the fibroblast suspension into the dermal and subcutaneous layers as previously described, into the skin  
10 above the lips at the vermilion border. In addition, the vertical philtrum may also be injected. The suspension is subsequently injected into the deeper tissues of the lip, including the muscle, in the manner described for subcutaneous injection.

#### 15 F. SURGICAL PLACEMENT OF AUTOLOGOUSLY CULTURED DERMAL/FASCIAL FIBROBLAST STRANDS

In a preferred methodology utilized to augment or repair the skin and/or lips by the surgical placement of autologously cultured dermal and/or fascial fibroblast strands, a needle (the "passer needle") is selected which is  
20 larger in diameter and greater in length than the area to be repaired or augmented. The passer needle is then placed into the skin and threaded down the length of the area. Guide sutures are placed at both ends through the dermal or fascial fibroblast strand. One end of the guide suture is fixed to a Keith needle which is subsequently placed through the passer needle. The  
25 guide suture is brought out through the skin on the side furthest (distal point) from the initial entry point of the passer needle. The dermal or fascial fibroblast graft is then pulled into the passer needle and its position may be

adjusted by pulling on the distal point guide suture or, alternately, the guide suture closest to the passer needle entry point. While the dermal or fascial strand is held in place by the distal point suture, the passer needle is pulled backward and removed, thus resulting in the final placement of the graft following the final cutting of the remaining suture.

Generally, the fascial or dermal graft is placed into the subcutaneous layer of the skin. However, in some situations, it may be placed either more deeply or superficially.

If the area to be repaired or augmented is either smaller or larger than would be practical to fill with the aforementioned needle method, a subcutaneous "pocket" may be created with a myringotomy knife, scissors, or other similar instrument. A piece of dermis or fascia is then threaded into this area by use of guide sutures and passer needle, as described above.

#### 15 G. INJECTION OF CELLS OR OTHER SUBSTANCES INTO THE VOCAL CORDS OR LARYNX

Generally, it is not possible to inject cellular matter or other substances directly into the vocal cord epithelium due to its extreme thinness. Accordingly, injections are usually made into the lamina propria layer or the muscle itself.

Generally, lamina propria tissue (finely minced if required for injection), fibroblasts derived from lamina propria tissue, or gelatinous substances are utilized for injection. The preferable methodology consists of injection directly into the space containing the lamina propria, specifically into Reinke's space. Injection is accomplished by use of laryngeal injection needles of the smallest possible gauge which will accommodate the injectate without the use of extraneous pressure during the actual injection process.

This is a subjective process as to the overall "feel" and the use of too much pressure may irreparably damage the injected cells. The material is injected via a syringe with a needle ranging from 30 to 18 gauge, with the gauge of the needle being dependent upon such factors as the overall viscosity of the injectate and the type of anesthetic utilized. Preferably, needles ranging from 22 to 18 gauge and 30 to 27 gauge are used with general and local anesthesia, respectively. If required, several injections may be performed along the length of the vocal cord.

To medialize a vocal cord with autologously cultured fascial or dermal fibroblasts, the materials are preferably injected directly into the tissue lateral or at the lateral edge of the vocal cord. The fibroblasts may be injected into scar, Reinke's space, or muscle, depending upon the specific vocal cord pathology. Preferably, it would be injected into the muscle.

The procedure may be performed under general, local, topical, monitored, or with no anesthesia, depending upon patient compliance and tolerance, the amount of injected material, and the type of injection performed.

If a greater degree of augmentation is required, a "pocket" may be created by needle dissection. Alternately, laryngeal microdissection, using knives and dissectors, may be performed. The desired material is then placed into the pocket with laryngeal forceps, or directly injected, depending upon the size of the pocket, the size of the graft material, the anesthesia, and the open access. If the pocket is left open after the procedure, it is preferably closed with sutures, adhesive, or a laser, depending upon the size and availability of these materials and the individual preferences of the surgeon.

While embodiments and applications of the present invention have been described in some detail by way of illustration and example for

purposes of clarity and understanding, it would be apparent to those individuals whom are skilled within the relevant art that many additional modifications would be possible without departing from the inventive concepts contained herein.

**WHAT IS CLAIMED IS:**

1. A method for corrective surgery in a human subject of a defect being amenable to rectification by the augmentation of tissue subjacent to the defect comprising the steps of: a) retrieving a plurality of viable cells from the subject; b) culturing the viable cells in vitro; and c) placing an effective volume of the in vitro cultured cells into a tissue of the subject, the tissue being located in a position subjacent to the defect to be rectified.
2. The method of claim 1 wherein the in vitro cultured cells are placed in the tissue of the subject by a method selected from injection, engraftment, engraftment by threading and direct placement.
3. The method of claim 1 wherein the in vitro cultured cells are fibroblasts.
4. The method of claim 3 wherein said fibroblasts are derived from a tissue selected from the group consisting of dermis, fascia, and connective tissue.
5. The method of claim 1 wherein the in vitro cultured cells are adipocytes.
6. The method of claim 1 wherein the cultured cells are suspended in a collagen or modified collagen solution prior to injection.
7. The method of claim 1 wherein the cells are cultured in a collagen or modified collagen matrix.

8. The method of claim 7 wherein the cells and the matrix are placed in the tissue by injection.
9. The method of claim 7 wherein the cells and the extracellular matrix  
5 are placed in the tissue by engraftment.
10. The method of claim 1 wherein serum from the subject or serum-free medium is used for in vitro culture of the cells.
- 10 11. The method of claim 1 wherein the in vitro cultured cells are washed in phosphate-buffered saline before being placed into the tissue of the subject.
12. The method of claim 1 wherein the defect is selected from the group consisting of a rhytid, stretch mark, depressed scar, cutaneous depression,  
15 hypoplasia of the lip, and scarring from acne vulgaris.
13. The method of claim 12 wherein the defect is selected from the group consisting of a stretch mark, wrinkle, depressed scar, cutaneous depression, hypoplasia of the lip, prominent nasolabial fold, prominent melolabial fold,  
20 and scarring from acne vulgaris.

14. The method of claim 1 wherein the in vitro cultured cells are placed by injection into:

- a) the lower dermis;
- b) the middle dermis;
- 5 c) the upper dermis; or
- d) the subcutaneous region of the skin; or.
- e) any combination of the foregoing within the tissue and/or surrounding the tissue.

10 15. An in vitro produced extracellular matrix composition, which is either substantially pure or combined with cells embedded in the matrix and is obtained from the process comprising the steps of: a) culturing cells in vitro in a culture vessel for a time sufficient for the cells to produce extracellular matrix; b) separating the extracellular matrix from the culture vessel and in  
15 addition, if the composition is substantially pure, separating the extracellular matrix produced by the cultured cells from such cells; and c) collecting the extracellular matrix.

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16. A method for corrective surgery in a human subject of a defect being amenable to rectification by the augmentation of tissue subjacent to the defect comprising the steps of:

- 5                   a) retrieving a plurality of viable cells from the subject;
- b) culturing the cells in vitro in a culture vessel for a time sufficient for the cells to produce extracellular matrix;
- c) separating the extracellular matrix produced by the cells from the culture vessel;
- 10                  d) collecting the extracellular matrix; and
- e) placing the collected extracellular matrix into a tissue subjacent to the defect.

17. The method of claim 16 wherein the extracellular matrix is exposed to a hypotonic solution prior to being placed into the tissue subjacent to the defect.

18. A method for the long-term augmentation of subcutaneous or dermal tissue in a human subject which comprises:

- 20                  (a) providing a suspension of autologous, passaged dermal fibroblasts, substantially free of immunogenic proteins;
- (b) identifying a defect that is susceptible to amelioration by augmentation of the subadjacent subcutaneous or dermal tissue; and
- (c) injecting an effective volume of the suspension into the
- 25                  subadjacent tissue so that the tissue is augmented.

19 . The method of claim 18, wherein the defect is a rhytid, stretch mark, a depressed scar, a cutaneous depression of non-traumatic origin or an underdevelopment of the lip.

5 20. The method of claim 18, which further comprises the steps of:

(a) biopsying the dermis of the subject;

(b) passaging the dermal fibroblasts from the dermal biopsy in a culture medium comprising between 5% and 20% non-human serum, so as to provide dermal fibroblasts substantially free of adipocytes, keratinocytes and  
10 extracellular matrix;

(c) incubating the passaged dermal fibroblasts in a serum-free medium; and

(d) exposing the incubated fibroblasts to a proteolytic enzyme so as to suspend the fibroblasts.

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21. A device for repairing a dermal defect in a subject comprising

(a) a hypodermic syringe having a syringe chamber, a piston disposed therein, and an orifice communicating with the chamber;

20 (b) a suspension comprising:

(1) dermal fibroblasts derived from the subject, said fibroblasts being substantially free of cells other than fibroblasts and substantially free of proteins that are immunogenic in the subject, and

(2) a pharmaceutically acceptable carrier solution, said  
25 suspension being disposed in the chamber; and

(c) a hypodermic needle affixed to the orifice.

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22. A method of making a device of claim 21, comprising the steps of:

(a) biopsying the dermis of the subject;

(b) passaging the dermal fibroblasts from the dermal biopsy in a  
5 culture medium comprising between 5% and 20% of non-human serum,  
serum from the subject or serum-free medium, so as to provide dermal  
fibroblasts substantially free of cells other than fibroblasts;

(c) incubating the passaged dermal fibroblasts in a serum-free  
medium;

10 (d) exposing the incubated fibroblasts to a proteolytic enzyme so as  
to suspend the fibroblasts; and

(e) adding the suspended fibroblasts to an acceptable carrier  
solution so that a suspension is formed and placing said suspension into the  
syringe chamber.

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