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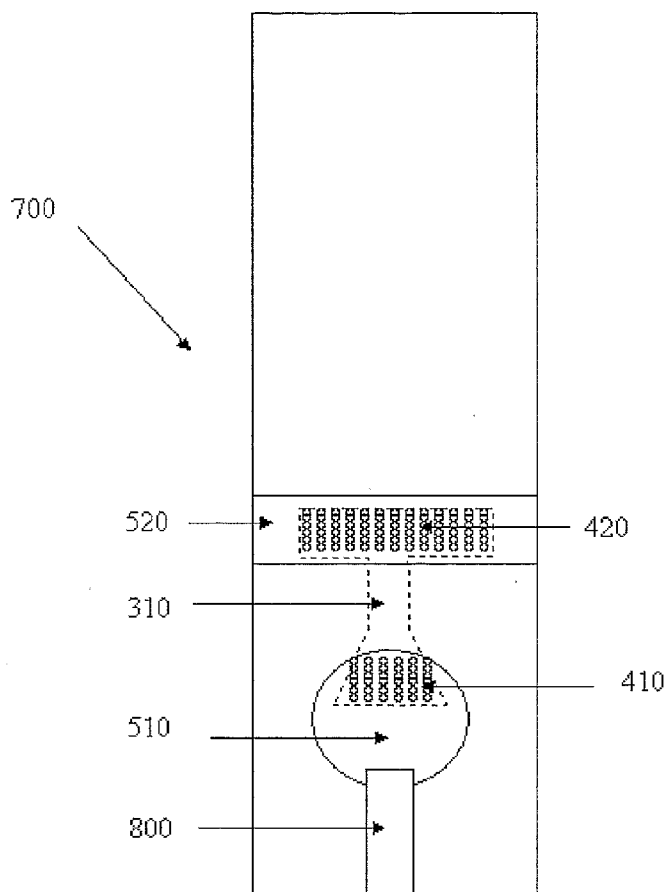
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[Continued on next page]

(54) Title: FLUID TRANSFER MECHANISM



(57) Abstract: A microfluidic device for transferring liquid from a first chamber to a second chamber is provided. The device has a first chamber; a second chamber; and a barrier between the first chamber and the second chamber, the barrier having at least one opening fluidly connecting the first chamber to the second chamber, the at least one opening being sized such that a retention force, such as surface tension, keeps the liquid in the first chamber. The fluid is transferred from the first chamber to the second chamber when an initiation input such as fluid pressure is introduced to the liquid that is sufficient to overcome the retention force. The device may be a sensor strip.

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FLUID TRANSFER MECHANISM

BACKGROUND OF THE INVENTION

Field of the Invention

[0001] The present invention relates generally to fluid transfer mechanisms.

Examples of particular embodiments of the invention relate to medical fluid testing mechanisms.

5 Related Art

[0002] The design of some sensor strips requires two or more chambers wherein fluid can be introduced into one chamber then transferred to a second chamber or additional chambers after a pre-determined time. In particular, immunoassay strips as disclosed in US Patent Application Nos. 10/830,841 and 11/284,097 had at least two chambers, a first reaction
10 chamber and a second detection chamber. In use, the liquid was first introduced into the reaction chamber and held there for a predetermined time while immuno-binding reactions proceeded, then transferred to the detection chamber. This timed transfer was achieved by having the detection chamber opening to the reaction chamber but unvented initially, such that when the reaction chamber filled, the opening to the detection chamber was closed off by the liquid. This
15 trapped air in the detection chamber prevented it from filling with liquid. When it was desired to fill the detection chamber, a vent was opened at the end of the detection chamber remote from the reaction chamber, usually by puncturing a layer, whereupon liquid transferred from the reaction chamber to the detection chamber either partially emptying the reaction chamber or drawing sample from a filling reservoir.

20 [0003] The method given above has a number of potential disadvantages. It can be difficult to close the entrance to the detection chamber in a reliable manner across the range of viscosities of samples encountered when testing whole blood. This means that differing amounts

of liquid can enter the detection chamber during filling of the reaction chamber, which can add to the variability of the response. Also, the reliability of a puncturing method can be difficult to guarantee over the life of a meter, with the potential for a needle or blade to become blunt with repeated use. It would therefore be desirable to develop a method for affecting a timed liquid
5 transfer that overcomes these difficulties.

BRIEF SUMMARY OF THE INVENTION

[0004] An example of an embodiment of the invention seeks to provide a reliable and robust method for transferring small volumes of liquid between chambers utilizing passive
10 transfer forces. The method involves providing a porous wall between the chambers between which the liquid is to be transferred. The porous wall has pores that are large enough to be substantially filled with the liquid to be transferred, but small enough such that the surface tension of the liquid interface with the second chamber prevents the liquid leaking out of the pores into the second chamber until an initiation step is performed.

15 [0005] Liquid is introduced into a first chamber such that it wets the porous wall and at least partially fills the pores. The liquid does not, however, enter the second chamber at this point as surface tension prevents it from exiting the opposite face of the porous wall into the second chamber. When it is desired to transfer liquid to the second chamber, an initiation step is performed which overcomes or breaks the surface tension and allows liquid to flow out of the
20 pores and into the second chamber.

[0006] The initiation step is such that it overcomes the surface tension holding the liquid in the pores in the wall and allows the liquid to enter the second chamber. This initiation step can be provided by supplying a pressure pulse to the liquid in the first chamber, creating a

vacuum in the second chamber, vibrating the strip, touching a surface to the surface of the porous wall facing the second chamber, or any other method that breaks or overcomes the surface tension.

[0007] Multiple second chambers can be filled from a single first chamber at the

5 same or at different times by inducing the initiation mechanism in the desired second chamber(s) at the desired time(s). In addition, a third chamber could be filled from the second chamber by having at least a portion of a wall of the second chamber porous and in common with the third chamber, with the initiation step being performed on the third chamber when the transfer is required. This can of course be repeated for a subsequent string of chambers in parallel or series.

10 [0008] Particular embodiments of the invention provide a fluid transfer device for transferring liquid from a first chamber to a second chamber. The device has a first chamber; a second chamber; and a barrier between the first chamber and the second chamber, the barrier having at least one opening fluidly connecting the first chamber to the second chamber, the at least one opening being sized such that a retention force keeps the liquid in the first chamber.

15 The fluid is transferred from the first chamber to the second chamber when an initiation input is introduced to the liquid that is sufficient to overcome the retention force.

[0009] Other embodiments of the invention provide methods of transferring liquid from a first chamber to a second chamber. The methods include providing a first chamber; providing a second chamber; providing a barrier between the first chamber and the second

20 chamber, the barrier having at least one opening fluidly connecting the first chamber to the second chamber, the at least one opening being sized such that a retention force keeps the liquid in the first chamber; and transferring the liquid from the first chamber to the second chamber.

The transferring takes place when an initiation input is introduced to the liquid that is sufficient to over come the retention force.

BRIEF DESCRIPTION OF THE DRAWINGS

- 5 [00010] The foregoing and other features and advantages of the invention will be apparent from the following, more particular description of particular embodiments of the invention, as illustrated in the accompanying drawings wherein like reference numbers generally indicate identical, functionally similar, and/or structurally similar elements.
- [00011] Figure 1 shows an example of a first embodiment of the invention;
- 10 [00012] Figure 2 is a sectional view along section line A-A' of the embodiment shown in Figure 1;
- [00013] Figure 3 is a sectional view along section line B-B' of the embodiment shown in Figure 1;
- [00014] Figure 4 shows an example of a second embodiment of the invention;
- 15 [00015] Figure 5 is a sectional view along section line A-A' of the embodiment shown in Figure 4;
- [00016] Figure 6 is a sectional view along section line B-B' of the embodiment shown in Figure 4;
- [00017] Figure 7 shows an alternate embodiment of the invention;
- 20 [00018] Figure 8 shows an example of a third embodiment of the invention;
- [00019] Figure 9 is an exploded view of the embodiment shown in Figure 8;
- [00020] Figure 10 is a graph showing current as a function of time of a first example of the invention; and

[00021] Figure 11 is a graph showing current as a function of time of a second example of the invention.

DETAILED DESCRIPTION OF THE INVENTION

5 [00022] The invention will now be described with reference to a specific two chamber embodiment with a specific initiation step. This embodiment relates to a disposable immunoassay strip using electrochemical detection of the results of an immuno-binding reaction. Note that the terms upper and lower are used for convenience only in the following description, they do not imply anything about the preferred orientation of the device during use, which can in
10 fact be used in any orientation.

[00023] The strip comprises three chambers, a filling chamber, a reaction chamber and a detection chamber. The filling chamber serves to receive the sample and act as a sample reservoir, the reaction chamber contains reagents whereby a probe is selectively immobilized in the reaction chamber to differing extents dependent upon the presence or concentration of an
15 analyte in the sample. The detection chamber contains electrodes and reagents so as to be able to detect the amount of probe transferred with liquid from the reaction chamber and thus detect or quantify the amount of analyte in the original sample. An example of such a strip is shown in Figures 1-3. The strip 100 has a number of layers which are laminated together using adhesives. The strip has three chambers, a filling chamber 1, a reaction chamber 2, and a detection
20 chamber 3. Layers 10 and 70 are sealing layers that serve to close the faces of chamber 1 to help to form a capillary space. Layer 20 is a layer carrying an electrically conductive upper surface which serves as an electrode in detection chamber 3. Layers 30 and 50 are spacer layers which

have adhesive upper and lower faces. Layers 30 and 50 serve to hold the laminate together and to define the height of the detection and reaction chambers, respectively. A region cut-out of layer 30 shown in Figures 2 and 3 defines the area of detection chamber 3 and the area of the detection chamber electrodes. A region cut-out of layer 50 shown in Figures 2 and 3 defines the area of reaction chamber 2. Layer 40 is a layer containing pores which serve as pores that connect reaction chamber 2 to detection chamber 3. Layer 40 has an electrically conductive coating on its lower surface that serves as the second electrode in detection chamber 3. Layer 60 serves to close reaction chamber 2 and filling chamber 1. Optionally, layer 60 can carry an electrically conductive coating on its lower surface to serve as an electrode to detect when liquid fills reaction chamber 2. With this option, liquid fills reaction chamber 2 and the pores in 40, thus bridging the electrode on the lower face of 40 and that on the lower face of 60. This bridging can be detected to tell the meter to initiate the test sequence. Layers 10 and 70 can be secured to layers 20 and 60, respectively, by any suitable method. A preferred method is to use adhesive. In one embodiment, the adhesive can be applied to the lower surface of layer 20 and the upper surface of layer 60, layers 10 and 70 can then be laminated to these adhesive layers. Alternatively, adhesive can be coated on to layers 10 and 70 and then those layers laminated to 20 and 60.

[00024] Figures 4-6 show an alternative embodiment where the cut-out in layer 50 to form reaction chamber 2 is such that the walls of the cut-out fully surround the cut-out to form an enclosed area. This embodiment has the advantage of preventing liquid from reaction chamber 2 wetting around the open edge of reaction chamber 2 to fill detection chamber 3 from its open edge, rather than through the porous wall connecting the two chambers. In this embodiment, the air that is displaced as liquid fills reaction chamber 2 can vent through the

holes in the porous wall, allowing the chamber to fill until all the pores in the wall are filled with liquid or reaction chamber 2 is fully filled. Note that it is not necessary for reaction chamber 2 to be completely filled for correct operation, just that there is a sufficient volume of liquid in contact with the reagents in reaction chamber 2 to fill detection chamber 3.

5 [00025] Also shown in Figures 4-6 is an embodiment where layers 10 and 70 are not required and instead layers 20 and 60 are extended to form the end walls of filling chamber 1. Optionally, in this embodiment the conductive layer on the upper surface of 20 can be extended into filling chamber 1. If this is done, when liquid fills reaction chamber 2 and the pores of layer 40, electrical connection is made via the liquid between the conductive layer on 20 in filling
10 chamber 1 and the conductive layer on the lower surface of layer 40. This can be detected electrically as a drop in the resistance or a change in the voltage, or current flowing or capacitance between the conductive layers on 20 and 40. This can serve as a signal to the meter that liquid has filled detection chamber 3 and thus automatically initiate a pre-determined test sequence. Note that an advantage of this method is that the signal won't be detected until the
15 liquid in filling chamber 1 is of sufficient volume to touch the opening of reaction chamber 2 and start to fill the pores of layer 40. Similar to the method disclosed in US 6,571,651, herein incorporated by reference, the capillary dimension of filling chamber 1 is greater than that of reaction chamber 2, thus filling chamber 1 can empty to fill reaction chamber 2. So if filling chamber 1 is sized so as to have a volume at least equal to and preferably slightly greater than
20 reaction chamber 2, then the signal indicating that liquid has been introduced into the device will not be detected until there is sufficient liquid introduced for the device to function as intended. An additional advantage of this is that if at first not enough liquid is introduced into filling chamber 1, more can be added until enough is present without affecting the intended operation

of the device. When the fluid transfer is initiated between reaction chamber 2 and detection chamber 3, a second change in the electrical conditions between the conductive surfaces on 20 and 40 will occur, due to the wetting of the conductive layer on 20 in the area of detection chamber 3. This change can be used to confirm to the meter that the fluid transfer has been successfully accomplished. Note that in general the current signal arising from the area of the conductive layer on 20 exposed in filling chamber 1 will be small compared to that generated by the area of the conductive layer exposed in detection chamber 3, so it will not interfere significantly with the signal from detection chamber 3. This is so as, in general, there are low concentrations of, or no significant amount of, electroactive species in the native sample that can generate current at the voltages normally applied between the electrodes in detection chamber 3. Also, the relatively long liquid path between the conductive layer exposed in filling chamber 1 and the conductive layer on 40 gives a relatively high electrical resistance, which tends to reduce the current signal produced.

[00026] An advantage of this embodiment is that only two electrical connections are required to detect all the electrical signals from the strip to complete the test, one connection to the conductive layer on 20 and the second to the conductive layer on 40. Suitable connectors for this are disclosed in US Patent Nos. 6,379,513 and 6,946,067, and in US Patent Application No. 11/284,136, which are incorporated by reference in this disclosure.

[00027] An alternative electrical connection method for this device is shown in Figure 7. The connection device 200 is illustrated with reference to the present invention, however it is to be understood that this aspect of the invention is applicable to any device when it is desired that connection be made to surfaces that are in close proximity and face one another. The numbered elements in Figure 7 with numbers common to the other figures denote the same

element in the present illustration. In this embodiment of this aspect of the invention, Figure 7 shows the end of the strip opposite to the end onto which filling chamber 1 opens. According to this embodiment, layer 20 is extended beyond spacer layer 30 and layer 40. Layer 20 carries an electrically conductive layer 70 on its upper surface and layer 40 carries an electrically

5 conductive layer 90 on its lower surface. It is desired to make separate electrical connection to layers 70 and 90. Layer 40 is extended beyond spacer layer 30. An additional layer 110 is introduced into the space between layers 20 and 40 that extends beyond 30. Preferably the thickness of layer 110 plus a conductive layer 80 and any adhesive layers that may be present is to equal to or slightly greater than the thickness of layer 30. Layer 110 is electrically conductive

10 at least on its upper surface 80 however is not electrically conductive through its full thickness, such that electrical connection can be made between 80 and 90 but not between 90 and 70 via 110. Layer 110 and conductive layer 80 carried thereupon extend beyond the edge of 40, thus by bringing 80 and 90 into electrical connection, electrical connection can be made to 90 via 80 in the area of 80 that extends beyond 40. Preferably an adhesive layer is present between the lower

15 surface of 110 and 70 to fix layer 110 in position. A conductive adhesive can optionally be placed between layers 90 and 80, in at least a portion of where they overlap, to help ensure good electrical connection. Alternatively the port containing the pins or similar devices to connect the strip to an external electrical circuit can be configured such that when the strip is inserted into the port, a face or faces of the port push against the upper surface of 40 to push 90 into

20 connection with 80.

[00028] An embodiment of the invention using a device with three active chambers is shown in Figures 8 and 9. Figure 8 shows a top view of a device with three active chambers and a filling chamber. Figure 9 shows an exploded view of this embodiment showing the various

layers. The strip 700 comprises a filling chamber 800, a first reaction chamber 510, a transfer and reaction chamber 310 and a second reaction chamber 520. Perforations 410 in layer 400 serve to connect first reaction chamber 510 with transfer and reaction chamber 310. Perforations 420 in layer 400 serve to connect transfer and reaction chamber 310 with second reaction chamber 520. In use, sample is added to filling chamber 800 until it fills to the opening to 510 at the end of filling chamber 800, whereupon the sample fills first reaction chamber 510. The air that is necessarily displaced during this filling process will vent through the open ends of second reaction chamber 520, via perforations 410 and 420. One or more reagents and reagent layers can be dried into first reaction chamber 510 to do a sample pre-treatment step, for example.

After the desired time in first reaction chamber 510, the transfer of fluid to transfer and reaction chamber 310 can be initiated by the means disclosed, such as pushing on layer 200 from below until it contacts the lower surface of layer 300 at the perforated area 410. When this is initiated, treated sample will flow from first reaction chamber 510 to fill transfer and reaction chamber 310 until perforations 420 are blocked with liquid sample such that air can no longer vent through perforations 420. Optionally, a second set of reagents can be dried into transfer and reaction chamber 310 if desired to perform a second reaction of the sample, such as a binding reaction as discussed below. Note that is it advantageous, but not necessary, for reactions to take place in all chambers. For example, first reaction chamber 510 could correspond to the reaction chamber of the embodiment shown in Figures 1-7 and second reaction chamber 520 could function as the detection chamber. In this case, transfer and reaction chamber 310 acts purely as a transfer chamber which separates first reaction chamber 510 and second reaction chamber 520 laterally as well as by perforated area 420. This can be advantageous in some applications in

minimizing vapor from the fluid in first reaction chamber 510, when filled, from diffusing to second reaction chamber 520 and wetting the reagents prematurely.

[00029] After the sample fluid is present in transfer and reaction chamber 310 for the desired time, a further transfer of sample from transfer and reaction chamber 310 to second
5 reaction chamber 520 can occur via perforations 420. This transfer can be initiated, for example, by pushing on the upper surface of layer 600 above perforations 420 such that the lower surface of layer 600 comes into contact with at least some of perforations 420. Further reagents can be dried into second reaction chamber 520 to further treat or react with components of the sample. For example, the results of any reactions carried out in transfer and reaction chamber 310 and
10 first reaction chamber 510 can be detected in second reaction chamber 520 and converted into a usable signal, either optical, electrochemical or for some other suitable method.

[00030] Figure 9 gives more detail of how the various chambers in this embodiment are formed. Layers 200 and 600 are the lower and upper closing layers, respectively, whose functions are to close faces of the capillary spaces in the strip, provide layers to contact the
15 perforated layer to initiate fluid transfer if initiation is performed in this manner, and to serve as supports on to which one or more other layers may be placed. Examples of other layers are layers of conductive material to form electrodes and electrical connection tracks and dried reagent layers that may be required to process the sample in the various chambers.

[00031] Layer 500 is an upper spacer layer. Portions of layer 500 are either cut away
20 or otherwise formed to define the area of first and second reaction chambers 510, 520. Layer 500 can be formed from a substrate with adhesive coated on both sides or may be just a layer of adhesive that has been formed or laid down with the areas that will correspond to first and second reaction chambers 510, 520 left free of adhesive. If an adhesive coated substrate is used,

the areas corresponding to first and second reaction chambers 510, 520 could be formed by punching or otherwise removing those areas.

[00032] Layer 400 is a layer that acts as a barrier between, and comprises the perforations necessary to complete the fluid transfers between, first reaction chamber 510 and transfer and reaction chamber 310 and transfer and reaction chamber 310 and second reaction chamber 520 when required. The perforations can be formed as described elsewhere in this disclosure. Layer 300 is a second spacer layer with an open area that serves to define transfer and reaction chamber 310. This can be constructed by the methods given above for layer 500. Filling chamber 800 can be formed by first laminating or otherwise joining layers 300, 400 and 500 with areas 310, 510 and 520 and perforations 410 and 420 pre-formed in the respective layers, and then punching through the tri-laminate to form the cut-out for filling chamber 800. Alternatively, the regions of 300, 400 and 500 that correspond to filling chamber 800 can be formed separately in the layers and then the layers laminated such that the cut-out regions align to form the side walls of filling chamber 800. The end faces of filling chamber 800 are closed when 200 and 600 are laminated to the upper and lower surfaces of the tri-laminate comprising 300, 400 and 500.

[00033] Referring to the embodiment illustrated in Figures 1-6, to function as a dry strip immunoassay, reagents can be dried into reaction chamber 2 and detection chamber 3 during fabrication. The reagents in reaction chamber 2 comprise a probe linked to a binding agent (hereafter termed the conjugate) and a binding target to which the binding agent can bind, where the species carrying the binding target, or the binding target itself, can be prevented from entering detection chamber 3. For example, the conjugate can consist of an enzyme such as PQQ dependent glucose dehydrogenase (GDH_{pqq}) linked to an antibody to an analyte of

interest. The target binding site can then be the analyte of interest tethered to magnetic beads.

The magnetic beads can be prevented from entering the detection chamber by means of a magnet

confining them to reaction chamber 3. Alternatively, the beads need not be magnetic but be

large enough such that they cannot fit through the pores in layer 40, such that this prevents them

5 from entering detection chamber 3. When there is analyte in the sample, the free analyte can

bind to the binding site on the conjugate and therefore block the conjugate from binding to the

immobilized target sites. The conjugate therefore remains free in solution and so able to transfer

to detection chamber 3. In this embodiment it is desirable that the conjugate and the target

binding site are not mixed before the sample contacts the reagents. To achieve this, the

10 conjugate can be dried onto the lower face of 60 and the species carrying the target binding sites

onto the upper face of 40. If the target binding sites are located on magnetic beads a permanent

or electromagnet placed next to the upper face of 60 can draw the beads up to mix with the

conjugate after sample has filled reaction chamber 2 and freed the magnetic beads from the

initially dry layer. In addition, the magnet serves to prevent the beads entering detection

15 chamber 3.

[00034] Detection chamber 3 also contains reagents dried down during strip

fabrication. These reagents are those necessary to translate the presence of the probe into a

current that can flow between the electrodes in detection chamber 3. In this embodiment of the

invention where the probe is an enzyme, a substrate and electrochemically active mediator for

20 the enzyme can be incorporated. Alternatively, the substrate for the enzyme can be incorporated

into reaction chamber 2. This has advantages where the substrate can take some time to become

active. When the probe is GDH, glucose is a suitable substrate, however the GDHpqq is only

active with β -D-glucose. D-glucose in the dried state is predominately in the form of α -D-

glucose, which proceeds to mutarotate to β -D-glucose once it dissolves. Thus it is advantageous to dissolve the glucose in the sample in reaction chamber 2 so that it can mutarotate while the binding reactions are taking place.

[00035] Any fluid containing a probe that enters the detection chamber will dissolve
5 the dried chemicals and the chemicals and the probe begin to react. In the case of GDHpqq as the probe, glucose is a suitable substrate and ferricyanide is a suitable mediator. When GDHpqq, glucose and ferricyanide are mixed the GDHpqq will oxidize the glucose and be reduced in the process, the GDHpqq will then be reoxidised by ferricyanide, which forms ferrocyanide in the process. The ferrocyanide can then be oxidized at the anode in the detection
10 chamber to produce a measurable current. This current can be related to the rate of production of ferrocyanide, which in turn can be related to the concentration of GDHpqq in the detection chamber, which in turn can be related to the concentration of analyte originally in the sample.

[00036] Optimally, the chemistry dried into the detection chamber should be dried onto the upper surface of 20. This prevents liquid filling the pores of 40 coming into contact
15 with the dried reagents prematurely. Additionally, the dissolving of the chemistry on 20 in the reacted sample liquid when the chemistry contacts the liquid filled pores of 40 (as set out below) helps to encourage the transfer of liquid into the detection chamber.

[00037] In order for the GDHpqq to be detected in the detection chamber liquid from the reaction chamber must be transferred to the detection chamber after a pre-determined time
20 when the binding reactions in the reaction chamber have proceeded to the desired point. When the liquid fills the reaction chamber, the hydrophilicity of the pores in 40 are such that they also fill with liquid at this point. However, for the liquid to exit the pores at the face of 40 facing the detection chamber it would have to increase the area of the air/liquid interface, which the liquid

surface tension opposes. Therefore the liquid tends to fill to the base of the pores and stop. In this embodiment, in order to break the surface tension layer 20 is pushed from below in the region of the detection chamber. This distorts 20 such that its upper surface comes into contact with the lower surface of 40. At the point(s) of contact, the liquid can now exit the pores in 40
5 without increasing the air/liquid interface area by directly wetting the upper face of 20.

However, as the pushing mechanism is withdrawn and the upper face of 20 moves away from the lower face of 40, the solution that wetted 20 moves away with it and draws more liquid through the pores of 40 in order to minimize the ratio of air/liquid interface to liquid volume as the surfaces move apart. This process draws liquid through the pores until eventually the

10 detection chamber is completely filled. Note that both the reaction chamber and the detection chamber should be open to the atmosphere when they are being filled for correct function, so that air can be displaced and vented during the filling processes. In the embodiment shown in Figures 1-3, a venting function is provided by the reaction and detection chambers opening to the sides of the strip 100. In the embodiment shown in Figures 4-6, the detection chamber is vented
15 through its openings to the sides of the strip and the reaction chamber is vented through the open sides of the detection chamber via the pores in 40.

[00038] Also, in order for this embodiment to function optimally it is desirable that the filling of the detection chamber does not result in the emptying of a chamber with similar capillary dimensions, as the two forces can oppose one another and create a slow or incomplete
20 fill. In the strip 100 shown, the filling chamber has a larger capillary dimension than either the reaction or the detection chamber. Thus when the detection chamber fills, the filling chamber will empty if there is no excess liquid attached to the filling chamber. Since the filling chamber has a larger capillary dimension than the detection chamber, the filling of the detection chamber

will be less impeded. Alternatively, if the filling chamber has the same capillary dimensions as the detection chamber then the detection chamber should be more hydrophilic than the filling chamber in order to affect the transfer of liquid. In general, the value of $(\gamma_{d,SL} - \gamma_{d,SA}) \Delta A_d + (\gamma_{f,SA} - \gamma_{f,SL}) \Delta A_f$ should be considered, where γ is the surface tension, ΔA is the change in the wetted area of a chamber, the subscripts d and f refer to the detection and filling chambers, respectively, SL refers to the solid-liquid interface and SA refers to the solid-air interface.

[00039] The invention has a number of advantages over the related art. A pusher mechanism rather than a piercing mechanism can be used to initiate fluid transfer, which should add robustness to the system. Also, the chambers can be stacked one upon the other, leading to miniaturization and manufacturing advantages. Also, multiple chambers can be stacked and offset, with multiple pusher mechanisms, as exemplified in Figures 8 and 9, thus allowing multiple chambers in either parallel or series to be filled as desired times, increasing flexibility. Also, electrode areas in the detection cell can be more conveniently defined since a cut-out region in 30 can entirely define the electrode areas.

[00040] Examples 1 and 2, below, are given as examples of embodiments of the invention and should not be considered as limiting in any way.

[00041] Example 1

[00042] 0.007 inch thick Melinex 329 was sputter coated with a thin layer of palladium to give an electrical resistance of 10 Ohms/sq to form layer 20. 0.002 inch thick Melinex 329 was coated with ca. 22 microns of heat activated adhesive ARCare-90503 (Adhesives Research Inc) on both sides to serve as layers 30 and 50. The adhesive tape was supplied with siliconised PET release liners on both faces.

[00043] A 0.004 inch thick web of PET was perforated by laser cutting through holes in lines in the down-web direction. The holes were conical in shape with the larger end being 150 micron diameter and the smaller end being 45 microns in diameter. The average hole density was 8.2 holes/mm². After perforation, one side of the web was sputter coated with gold to give an electrical resistance of 10 Ohms/sq.

[00044] The double sided adhesive tape was laminated to both sides of the perforated PET leaving the gaps as shown in Figure 1 which would form the reaction chamber 2 and the detection chamber 3. The palladium coated Melinex was then laminated to the lower face of layer 30 to form layer 20. Clear PET film was laminated to the upper face of layer 50 to form layer 60. Filling chamber 1 was then formed by punching through layers 20 to 60 and laminating adhesive coated PET film layers 10 and 70 to close the faces of filling chamber 1.

[00045] Conjugate and derivatised magnetic beads were prepared as per US Patent Application Publication No. US-2006-0134713-A1, herein incorporated by reference. The conjugate comprised an antibody to CRP (C-Reactive Protein) joined to at least one GDHpqq. The surface of the magnetic beads were modified to comprise CRP. This CRP served as the immobilized binding site for the conjugate. The magnetic beads were prevented from entering the detection chamber by a permanent magnet placed near the reaction chamber.

[00046] The conjugate was dried onto the lower face of layer 60. In some strips beads were dried on the upper face of layer 40. A mixture of potassium ferricyanide, glucose and buffer was dried on the upper surface of layer 20. During testing a permanent magnet was placed adjacent to the upper face of layer 60. This served the dual purpose of preventing beads (if present) entering the detection chamber and attracting the beads towards the layer of

conjugate to promote mixing of the two once the sample was introduced into the reaction chamber.

[00047] In use, sample was introduced into filling chamber 1 until it filled across to touch the entrance to reaction chamber 2, whereupon reaction chamber 2 also filled with sample.

5 Sixty seconds was then allowed to elapse. After sixty seconds, a metal rod was pressed against the lower surface of 20 such that 20 was deflected up until the upper surface of 20 came into contact with liquid filling the holes in layer 40, whereupon liquid flowed through the holes in 40 to completely fill detection chamber 3. When liquid bridged the space between the electrode on the upper face of 20 and that on the lower face of 40 the meter initiated an electrochemical test
10 sequence, where it made the lower electrode +300 mV relative to the upper electrode for 16 seconds.

[00048] Figure 10 shows plots of the typical current response for strips filled with 0.1 M HEPES buffer in water with and without the presence of CRP labeled beads in the test solution. When no beads are present, maximal conjugate should be transferred to detection
15 chamber 3. When an excess of CRP labeled beads over conjugate is present in the solution the conjugate is substantially immobilised on the beads leading to a minimal transfer of conjugate to detection chamber 3. In this case the lower electrode was at +300 mV with respect to the upper electrode during the sixteen seconds the potential was applied.

[00049] Figure 11 shows typical current responses for strips with conjugate and beads
20 dried into them when tested blood serum containing either zero or 250 micrograms/milliliter of CRP. In this case the upper electrode was at +300 mV with respect to the lower electrode.

[00050] Example 2

[00051] The invention is also pertinent to a sensor with a single, larger punched hole in layer 40 rather than a series of small, laser formed holes. For example, a 1.5 mm diameter male/female punch was used to create a hole in layer 40. When liquid filled chamber 2, it stopped just past the edge of the hole. When layer 20 was pushed against the hole, the liquid
5 entered chamber 3.

[00052] The invention is not restricted to the number of holes per sensor or the range of hole diameters described in Examples 1 and 2.

[00053] The invention is not limited to the above-described exemplary embodiments. It will be apparent, based on this disclosure, to one of ordinary skill in the art that many changes
10 and modifications can be made to the invention without departing from the spirit and scope thereof.

WHAT IS CLAIMED IS:

1. A fluid transfer device for transferring liquid from a first chamber to a second chamber, the device comprising:
 - a first chamber;
 - a second chamber; and
 - a barrier between the first chamber and the second chamber, the barrier having at least one opening fluidly connecting the first chamber to the second chamber, the at least one opening being sized such that a retention force keeps the liquid in the first chamber,wherein the fluid is transferred from the first chamber to the second chamber when an initiation input is introduced to the liquid that is sufficient to overcome the retention force.
2. The device of claim 1, wherein the retention force is surface tension of the liquid at the at least one opening.
3. The device of claim 2, wherein the initiation input is fluid pressure applied to the liquid in the at least one opening and in a direction from the first chamber to the second chamber.
4. The device of claim 2, wherein the second chamber has an inner surface and an outer surface, and
 - the initiation input is pressure applied to the outer surface of the second chamber such that the inner surface of the second chamber contacts the liquid in the at least one opening and causes the liquid to flow through the at least one opening into the second chamber.

5. The device of claim 1, wherein the device is a sensor strip,
the first chamber is a reaction chamber of the sensor strip, and
the second chamber is a detection chamber of the sensor strip.
6. The device of claim 1, further comprising
a third chamber; and
a second barrier between the second chamber and the third
chamber, the second barrier having at least one opening fluidly connecting the
second chamber to the third chamber, the at least one opening in the second barrier
being sized such that a second retention force keeps the liquid in the second
chamber,
wherein the fluid is transferred between the second chamber and
the third chamber when a second initiation input is introduced to the liquid that is
sufficient to over come the second retention force.
7. The device of claim 6, wherein the second retention force is surface
tension of the liquid at the at least one opening in the second barrier.
8. The device of claim 7, wherein the second initiation input is fluid
pressure applied to the liquid in the at least one opening in the second barrier and
in a direction from the second chamber to the third chamber.
9. The device of claim 7, wherein the third chamber has an inner
surface and an outer surface, and

the second initiation input is pressure applied to the outer surface of the third chamber such that the inner surface of the third chamber contacts the liquid in the at least one opening in the second barrier and causes the liquid to flow through the at least one opening in the second barrier into the third chamber.

10. The device of claim '6, wherein the device is a sensor strip,
the first chamber is a reaction chamber of the sensor strip,
the second chamber is a transfer and reaction chamber of the sensor strip, and

the third chamber is a reaction chamber of the sensor strip.

11. A method of transferring liquid from a first chamber to a second chamber, comprising:

providing a first chamber;

providing a second chamber;

providing a barrier between the first chamber and the second chamber, the barrier having at least one opening fluidly connecting the first chamber to the second chamber, the at least one opening being sized such that a retention force keeps the liquid in the first chamber; and

transferring the liquid from the first chamber to the second chamber,

wherein the transferring takes place when an initiation input is introduced to the liquid that is sufficient to overcome the retention force.

12. The method of claim 11, wherein the retention force is surface tension of the liquid at the at least one opening.

13. The method of claim 12, wherein the initiation input is fluid pressure applied to the liquid in the at least one opening and in a direction from the first chamber to the second chamber.

14. The method of claim 12, wherein the initiation input is pressure applied to an outer surface of the second chamber such that an inner surface of the second chamber contacts the liquid in the at least one opening and causes the liquid to flow through the at least one opening into the second chamber.

15. The method of claim 11, wherein the first chamber is a reaction chamber of a sensor strip, and

the second chamber is a detection chamber of the sensor strip.

16. The method of claim 11, further comprising
providing a third chamber;
providing a second barrier between the second chamber and the third chamber, the second barrier having at least one opening fluidly connecting the second chamber to the third chamber, the at least one opening in the second barrier being sized such that a second retention force keeps the liquid in the second chamber; and

transferring the liquid from the second chamber to the third chamber,

wherein the transferring between the second chamber and the third chamber takes place when a second initiation input is introduced to the liquid that is sufficient to overcome the second retention force.

17. The method of claim 16, wherein the second retention force is surface tension of the liquid at the at least one opening in the second barrier.
18. The method of claim 17, wherein the second initiation input is fluid pressure applied to the liquid in the at least one opening in the second barrier and in a direction from the second chamber to the third chamber.
19. The method of claim 17, wherein the second initiation input is pressure applied to an outer surface of the third chamber such that an inner surface of the third chamber contacts the liquid in the at least one opening in the second barrier and causes the liquid to flow through the at least one opening in the second barrier into the third chamber.
20. The method of claim 16, wherein the first chamber is a reaction chamber of a sensor strip,
the second chamber is a transfer and reaction chamber of the sensor strip; and
the third chamber is a reaction chamber of the sensor strip.

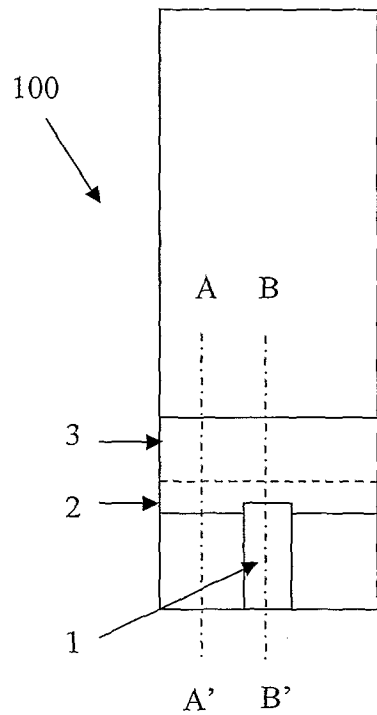


Figure 1

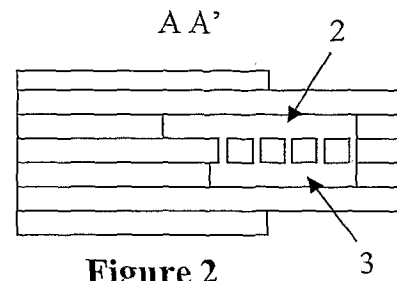


Figure 2

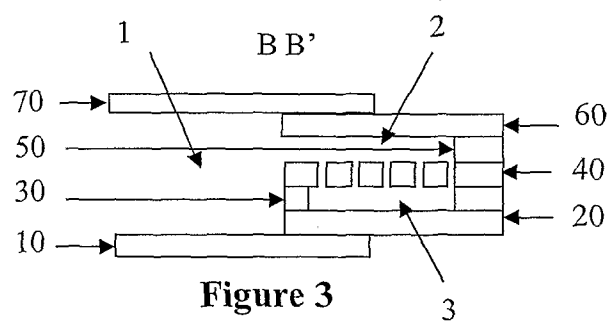


Figure 3

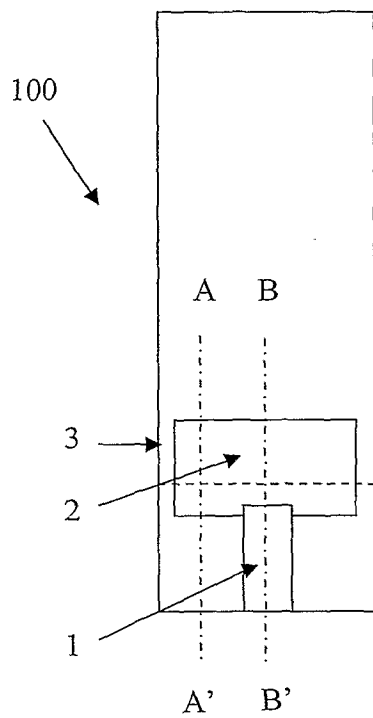


Figure 4

A A'

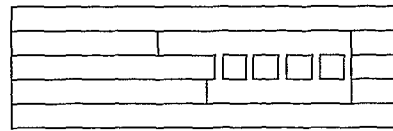


Figure 5

B B'

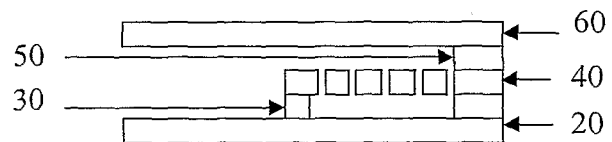


Figure 6

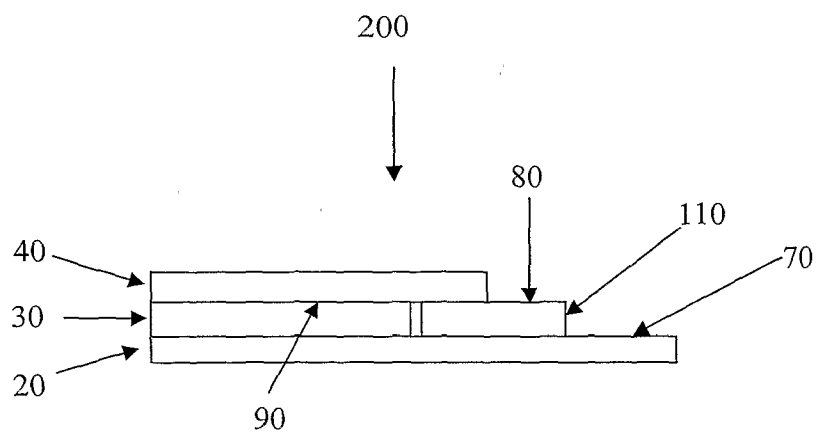


Figure 7

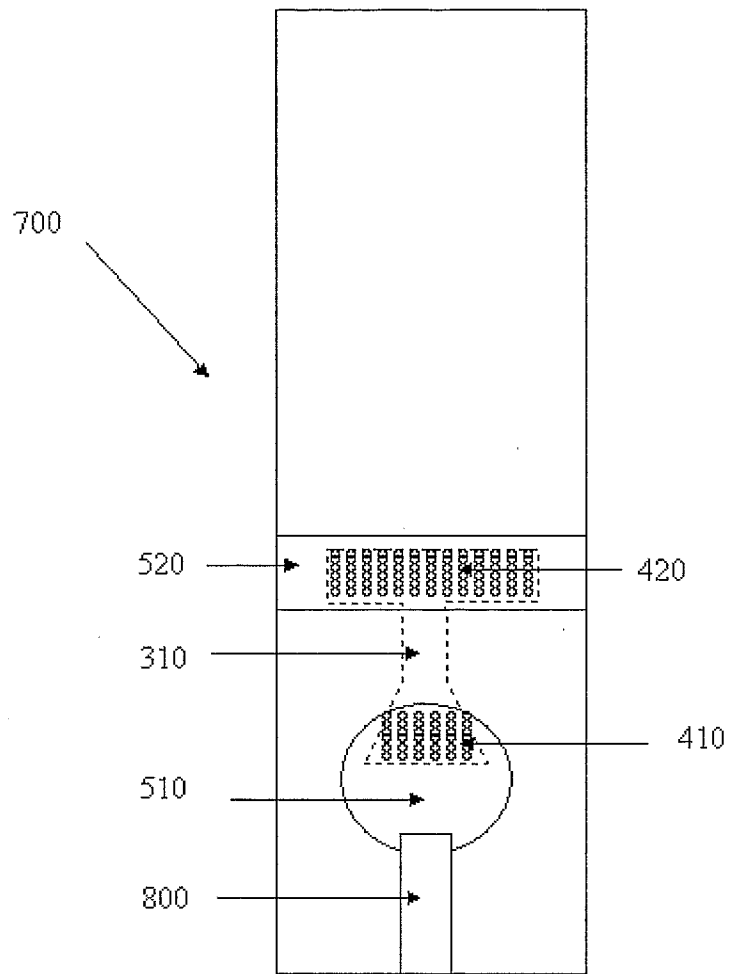


Figure 8

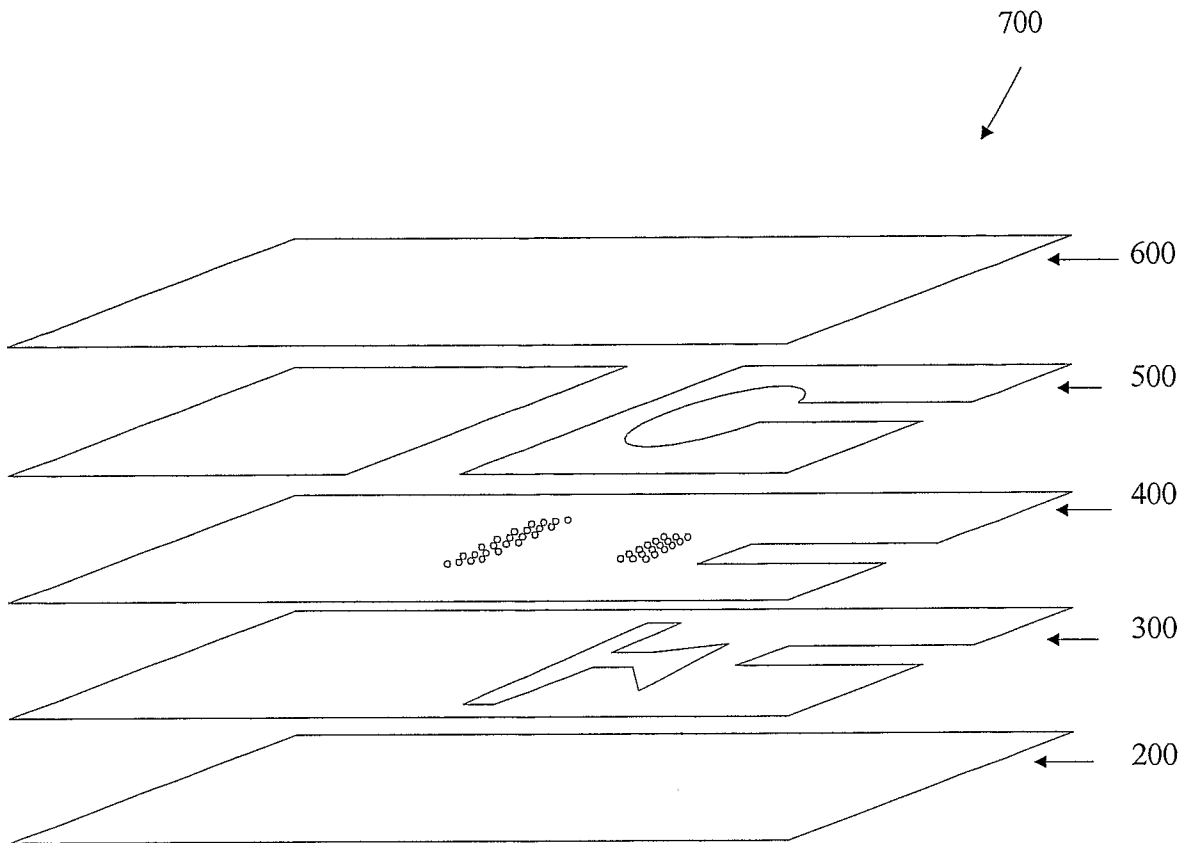


Figure 9

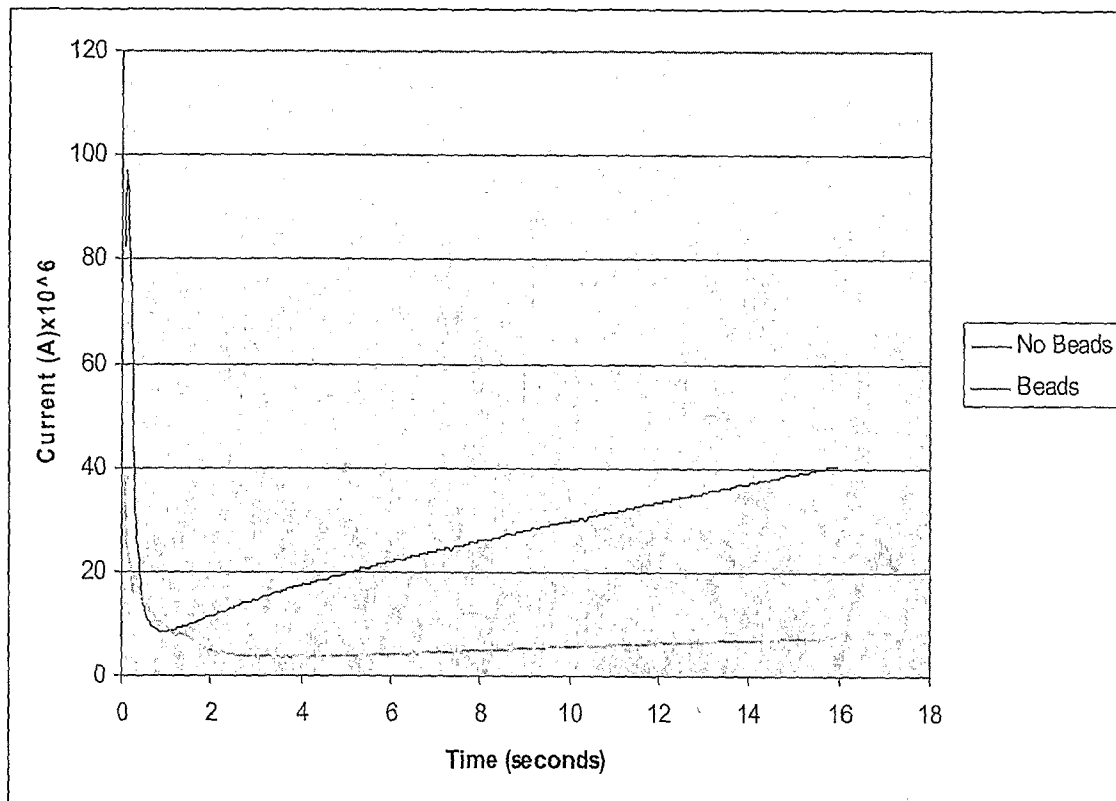


Figure 10

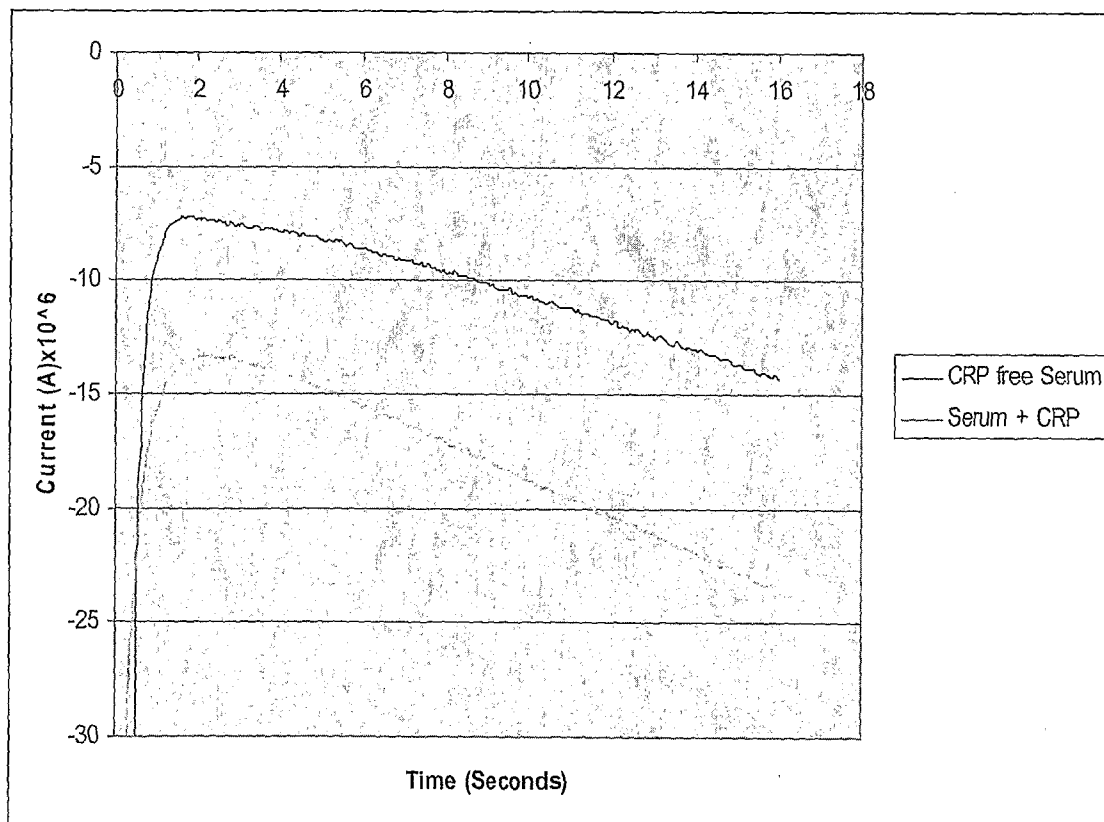


Figure 11

INTERNATIONAL SEARCH REPORT

International application No.

PCT/IB2007/000370

A. CLASSIFICATION OF SUBJECT MATTER

Int. Cl.

G01N 33/49 (2006.01) **B81B 1/00** (2006.01) **G01N 33/53** (2006.01)

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

DWPI: fluid, liquid, transfer, move, microfluid, surface, tension, pores, activate, assay, biosensor, chamber, well, reaction and similar terms

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2004/0121450 A1 (PUGIA ET AL.) 24 June 2004 See entire document especially Figures; Pages 1-3; Paragraph [0073]	1-20
X	WO 2005/093388 A1 (INFECTIO RECHERCHE INC.) 6 October 2005 See entire document especially Figures 1-5; Pages 4-6; Paragraphs [0009], [0032], [0052-0056]	1-3, 6-8, 11-13, 16-18
X	US 2004/0265172 A1 (PUGIA ET AL.) 30 December 2004 See entire document especially Figures; Paragraphs [0013-0016], [0021-0025], [0043]	1-3, 6-8, 11-13, 16-18



Further documents are listed in the continuation of Box C



See patent family annex

* "A"	Special categories of cited documents: document defining the general state of the art which is not considered to be of particular relevance	"T"	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E"	earlier application or patent but published on or after the international filing date	"X"	document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"L"	document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"Y"	document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"O"	document referring to an oral disclosure, use, exhibition or other means	"&"	document member of the same patent family
"P"	document published prior to the international filing date but later than the priority date claimed		

Date of the actual completion of the international search
10 May 2007

Date of mailing of the international search report 14 MAY 2007

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INTERNATIONAL SEARCH REPORT

International application No.

PCT/IB2007/000370

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 1999/058245 A1 (AMERSHAM PHARMACIA BIOTECH AB) 18 November 1999 See entire document especially Figures; Pages 1-5, 11	1-3, 11-13
X	US 2004/0091399 A1 (CHUNG ET AL.) 13 May 2004 See entire document especially Figures; Paragraphs [0012-26], [0032-0034]	1-2, 6-7, 11-12, 16-17
A	US 2005/0047972 A1 (LAUKS ET AL.) 3 March 2005 See entire document	1-20
A	WO 2001/035088 A1 (NEW MEXICO STATE UNIVERSITY TECHNOLOGY TRANSFER CORPORATION) 17 May 2001 See entire document	1-20

INTERNATIONAL SEARCH REPORT

International application No.

PCT/IB2007/000370

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report				Patent Family Member			
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		WO	2004061414				
WO	2005093388	CA	2559778	EP	1728062		
US	2004265172	CA	2530585	EP	1641566	WO	2005003724
WO	9958245	AU	36243/99	AU	2002243148	AU	2003224586
		CA	2333618	CA	2439627	CA	2441206
		CA	2442342	CA	2442345	CA	2455894
		CA	2456421	EP	1077771	EP	1384076
		EP	1384249	EP	1386343	EP	1390144
		EP	1427530	EP	1448473	EP	1483052
		EP	1525451	GB	2341924	GB	2350678
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		US	2005153433	US	2005153434	US	2005277195
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		WO	03035538	WO	03093802		
US	2004091399	KR	2004004176				
US	2005047972	CA	2576114	EP	1664725	WO	2005022123
WO	0135088	AU	22490/01	US	6878255		

Due to data integration issues this family listing may not include 10 digit Australian applications filed since May 2001.

END OF ANNEX