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(54) Title: TC AND RE LABELER RADIOACTIVE GLYCOSYLATED OCTREOTIDE DERIVATIVES

(57) Abstract: Improved sst-receptor binding peptidic ligands for diagnostic and therapeutic applications in nuclear medicine are provided. The improved ligands contain either natural or unnatural amino acids or peptidomimetic structures that are modified at either the N-terminal or the C-terminal end or at both termini, a carbohydrate unit and a chelator or prosthetic group to provide a complexation of a radioisotope binding or holding the radioisotope. The sst- or SSTR- receptor binding peptidic ligands may also contain one or more multifunctional linker units optionally coupling the peptide, and/or the sugar moiety and/or the chelator and/or the prosthetic group. Upon administering the ligand to a mammal through the blood system the ligand provides improved availability, clearance kinetics, sst-receptor targeting and internalization over the non-carbohydrated ligands.

Tc and Re LABELER RADIOACTIVE GLYCOSYLATED OCTREOTIDE
DERIVATIVES

5

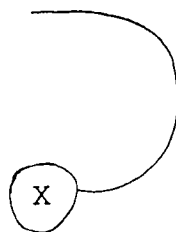
The present invention relates to novel radioactive octreotide derivatives that are glycosylated and bind the somatostatin receptor.

10 These so-called SSTR-ligands are suitable for the in vivo targeting of somatostatin receptors and find broad application in nuclear medicine.

Essential parts of these molecules are sugar moieties conjugated directly or via linkers to the bioactive part of the molecule. Compared to the
15 corresponding non-carbohydrated derivatives, these derivatives, labeled with radioisotopes such as Rhenium and Technetium, either via direct reductive methods or via tricarbonyl complexes, lead to potent somatostatin receptor ligands with improved tumor/non-tumor
20 accumulation ratios, improved pharmacokinetics and improved internalization kinetics.

The somatostatin receptor binding peptidic ligand of this invention are prepared from natural or unnatural (prepared) ligands. These ligands bear
25 structural modifications at the N-terminal end or the C-terminal end or both termini. Said peptide ligands have affinity to sst- receptors and are graphically represented by the structure:

30



35

wherein X indicates the C-terminus of the ligand. In the compositions of this invention wherein there may be multiple ligands where is permitted the formation of di-

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and multimers by mixed C- and N- terminal coupling of the peptide chain. Thus, the scope of this invention cover homo-, dimer, homomultimers or different receptor binding structures, heterodimers, and heteromultimers. The di- and multimers can be formed by mixed C-and N- terminal coupling of the peptide chain.

The ligand composition of this invention optionally contains at least one linker unit that can be multifunctional. Such linker unit allows coupling together of the peptide, sugar moiety, and chelator via a condensation-, acylation-, alkylation-, substitution- or addition reaction. Typical linker units comprise ligands taken from peptidic or other organic structures such as L- or D-amino acids such as lysine, ornithine serine, glutamic acid, aspartic acid, O-amine serine, mercaptopropionic acid, hydroxy carbonic acids, amino carbonic acids, halogen carbonic acids or polyamino acids.

The improved somatostatin receptor binding peptidic ligand of this invention comprises a carbohydrate, specifically a sugar such as a mono-, di- and trisaccharide. Typical suitable sugars include glucose, galactose, maltose, mannose, maltotriose and lactose coupled via covalent linkage. That is, the sugar can be combined via the Maillard reaction and Amadori rearrangement, glycosidic linkage, alkylation, allylation or coupled via complex formation after modification, that is, formation of carbohydrate isonitriles or carbohydrate phosphates.

Another component of the improved somatostatin receptor binding peptidic ligand of this invention is a chelator. Typical chelators are peptidic or non-peptidic structures suitable for mono- or multidentate complexation of radioisotopes of Tc and Re. The chelator useful in compositions of this invention comprise one or more (ligand and coligand(s)) organic molecules containing any number of functional groups necessary to the complexation of the radiometals, depending on its oxidation state and

complex geometry. Exemplary suitable chelators are, for example, histidine, picolylamine diacetic acid, hydroxy nicotine amide (HYNIC), mercaptoacetyl-glycyl-glycyl-glycine (MAG3) and tetrapeptides.

5 To more clearly describe the improved somatostatin receptor binding peptidic ligand of this invention, reference is made to Figs. 1A-1C. In Fig. 1A-1C there is shown, in graphical schematic form, the various configurations into which the peptide ligands of
10 this invention can be prepared. Other practical configurations may occur to those skilled in this art in keeping with the teaching of this specification.

In Fig. 1A, Fig. 1B and Fig. 1C there is shown mono-di- and multimers (wherein n is an integer of 2 or more)
15 containing a linker moiety, L sugar moiety, S and a chelator, C capable of holding a radioisotope of Tc and Re.

In Figs. 1A, 1B and 1C the termini of the peptide is designated by indicating the C- terminus by X, the opposite terminus being the N terminus. Thus the
20 pharmacophoric peptide is coupled with the C- or N-terminal end to the linker, chelator, etc. As indicated above, both the peptide ligand and the linker (multifunctional) can comprise natural or unnatural amino acids. Of course, the ligand (i.e. octreotide) will not
25 be employed as the linker in compositions of this invention.

In Fig. 1A there is shown various configurations of compositions of this invention providing multimers of peptide ligands of two or more. The multimers may
30 comprise either identical receptor peptide binding structures (homodimers, homomultimers) or different receptor binding structures (heterodimers, heteromultimers).

In Fig. 1B, there is shown various
35 configurations of mers some of which contain a linker unit (multifunctional) and four of which do not contain a linker unit. Thus it is seen that a multifunctional linker unit is optional in the compositions of this

invention.

In Fig. 1C, there is shown dimers and multimers wherein multiple linker units are employed with varying orientation of the peptide and, of course, multiple peptide ligands.

5 The dimers and multimers shown in Figs 1A and 1C can be formed via covalent linkage of the linker or the peptide ligand to the chelator or formation of a complex between the linker and the chelator.

Thus, the present invention provides a somatostatin receptor (sst) binding peptidic ligand comprising natural or unnatural amino acids or a peptidomimetic structure, at least one carbohydrate and at least one chelating group allowing
10 mono- or multidentate complexation of a radioisotope selected from Tc and Re.

The invention is described in is illustrated in the non-limiting examples that follow.

15 **EXAMPLES**

EXAMPLE 1

**Rational design of peptide radiopharmaceuticals: in vitro studies demonstrate a synergistic effect of carbohydrate and C-terminal oxidation
20 of octreotide on ligand induced SST-₂ internalization.**

Aims: Besides by its pharmacokinetics, the suitability of a receptor based tracer for imaging and therapeutic purposes is mainly determined by its pharmacodynamic profile. Aim of this study was to investigate the effect of carbohydrate of octreotide and octreotate on SSTR endo- and exocytosis
25 (internalization and externalization) and reendocytosis (recirculation).

Methods: Internalization, externalization and recycling of [¹²⁵I]Tyr³-octreotide (TOC), [¹²⁵I]Tyr³-octreotate (TOCA) and their Glucose- (Gluc) and Maltotriose- (Mtr) derivatives were studied using confluent monolayers of AR42J-cells (SSTR₂). The cells were incubated with the radioligand for up to 120 min (n=3). At each time
30 point the activity in the supernatant, the surface-bound and the internalized activity were determined and normalized to the values of TOC. Externalization and recycling was studied after an incubation time of 120 min

over 2h. Specificity of ligand binding was studied in a competition experiment with 10 μ M Sandostatin.

Results: After 2h of incubation the amount of internalized ligand [% internalized TOC] was as follows:
5 Mtr-TOC(35 $\pm$ 4%) <Gluc-TOC(121%) <TOCA(154%) <Mtr-TOCA (549%) <Gluc-TOCA (637%). In the competition experiment internalization of all compounds dropped to < 0.1 $\pm$ 0.02% (30 min) of the applied radioactivity. In the
10 externalization experiment that allowed recycling of the ligands, TOCA and glycated TOCA's showed about 2/3 of extracellularly located radioactivity compared to the experiment without recycling, while about 80% were found for TOC, Gluc-TOC and Mtr-TOC. Carbohydratation of TOC had no significant effect on the availability of the ligands
15 on the cell surface, whereas surface concentration of TOCA and Mtr-TOCA is increased by a factor of 2.1 and 2.3 respectively compared to TOC. Gluc-TOCA shows a fivefold increase of the availability of the tracer on the cell surface compared to TOC. The internalization rate
20 (internalized /surface bound act.) of TOC is not significantly affected by glycosylation, whereas TOCA shows a 1.4 fold increase. For Gluc-TOCA and Mtr-TOCA we observed internalization rates of 186 and 171% compared to TOC.

25 Conclusion: Using AR42J-cells, carbohydratation of TOCA led to a significant increase in cell surface concentration and internalization rate of the radioligands.

30 **EXAMPLE 2**

CARBOHYDRATED TC-99M-OCTREOTIDE DERIVATIVES FOR SPECT SYNTHESIS, RADIOLABELLING AND IN VIVO DATA

Over the past decade different approaches to ^{99m}Tc -
35 and ^{18}F -labelled octreotide derivatives for SSTR-scintigraphy using SPECT and PET have been investigated. Decristoforo et al. showed that ^{99m}Tc -labelled HYNIC-Tyr³-octreotide with EDDA as a coligand has favourable

biokinetics and high tumor uptake in mice.

2-[¹⁸F]fluoropropionyl-D-Phe¹-octreotide, the only ¹⁸F-labelled octreotide analog known so far, shows predominant hepatobiliary excretion, which is one drawback with
5 respect to its application for in vivo SSTR-imaging.

The inventors found that N-terminal glycosylation of radioiodinated Tyr³-octreotide (TOC) and its Thr⁸-derivative Tyr³-octreotate (TOCA) leads to a significant improvement of the biodistribution, i.e. to an increased
10 tumor accumulation. To investigate the general applicability of this principle, we synthesized and evaluated glycosylated octreotide- and octreotate-derivatives for ^{99m}Tc- labelling (Figure 2).

N-glycosylated derivatives of Lys⁰(N-His)-TOC (K⁰(H)TOC)
15 were used as precursors for ^{99m}Tc-labelling using the organometallic aquaion [^{99m}Tc(H₂O)₃(CO)₃]⁺-approach [1]. The peptide was synthesized according to a standard Fmoc-SPPS protocol. Conjugation with glucose (Gluc) and maltotriose (Mtr) was performed via Amadori reaction.
20 ^{99m}Tc-labelling of the Lys⁵-deprotected peptides yielded [^{99m}Tc]Gluc-K⁰(H)TOC and [^{99m}Tc]Mtr-K⁰(H)TOC with radiochemical yields > 97% based on the aquaion.

Biodistribution studies of the ^{99m}Tc-labelled
25 derivatives (30 and 120 min p.i.) were performed in AR42J-tumor bearing nude mice (n=3-4). Internalisation- and externalisation experiments were carried out using the same cell line.

An increase of internalisation was found for
30 [^{99m}Tc]Gluc-K⁰(H)TOC by a factor of 2.3±0.8 and for [^{99m}Tc]Mtr-K⁰(H)TOC by a factor of 3.6±0.4 compared to the reference [¹²⁵I]TOC. While [¹²⁵I]TOC is rapidly externalised from the cell upon incubation, [^{99m}Tc]Gluc-K⁰(H)TOC remains trapped within the cell up to 120 min.

35 The biodistribution of [^{99m}Tc]Gluc-K⁰(H)TOC and [^{99m}Tc]Mtr-K⁰(H)TOC 2 h p.i. are shown in Table 1.

Table 1

Tissue
accumulation
[%ID/g]
Of [^{99m}Tc]Gluc-
 $\text{K}^0(\text{H})\text{TOC}$
And [^{99m}Tc]Mtr-
 $\text{K}^0(\text{H})\text{TOC}$
In AR42J tumor
bearing
Nude mice 2 h
p.i. (n=3-4)

	[^{99m}Tc]Gluc- $\text{K}^0(\text{H})\text{TOC}$	[^{99m}Tc]Mtr- $\text{K}^0(\text{H})\text{TOC}$
blood	1.49 ± 0.18	4.12 ± 0.87
liver	15.89 ± 2.70	14.34 ± 1.55
intestine	2.83 ± 0.28	2.02 ± 0.41
stomach	11.28 ± 2.74	6.22 ± 0.75
kidney	19.49 ± 2.22	17.97 ± 2.76
muscle	0.22 ± 0.04	0.40 ± 0.10
adrenals	6.47 ± 1.46	4.94 ± 0.38
pancreas	6.43 ± 2.09	3.32 ± 0.38
tumor	12.21 ± 0.96	14.02 ± 6.33

- Both glycosylated compounds show high accumulation in sst₂ positive tissue 120 min p.i.. We suppose that the comparatively high non-specific uptake in excretion organs as well as a delayed blood clearance are due to the insufficient complexation of the ^{99m}Tc -core by the bidentate histidine ligand. The remaining metal coordination site may be saturated by thiol-containing native proteins in vivo, which can result in rapid trapping of these complexes in the blood, the liver and other excretion organs. The formation of saturated complexes of the [$^{99m}\text{Tc}(\text{H}_2\text{O})_3(\text{CO})_3$]⁺-aquaion with tridentate ligands such as N-Ac-His result in a significant decrease of activity accumulation in non-tumor tissue.
- It can be concluded, that the introduced tracer design based on the combination of carbohydrate conjugation of octreotide(-tate) and of tridentate complexation of the [$^{99m}\text{Tc}(\text{H}_2\text{O})_3(\text{CO})_3$]⁺-aquaion is the basis of a new series of very promising SSTR-tracers.

¹ Egli A. et al. *J.Nucl.Med.* 40: 1913-1917 (1999)

EXAMPLE 3**GLYCATION OF SST-RECEPTOR-AGONISTS: IMPROVEMENT OF DYNAMIC LIGAND TRAFFICKING OF RADIOLABELLED SOMATOSTATIN AGONISTS**

Carbohydration is now found to be a powerful tool to improve the pharmacokinetics of radiolabelled octreotide and V_{V33} analogs. Glycation of octreotide and octreotate significantly reduces hepatobiliary excretion and kidney uptake and enhances tumor uptake and tumor/tissue ratios. Tumor accumulation of a radiolabelled ssr_2 -agonist relies upon the dynamic processes of receptor mediated internalisation, degradation and subsequent intracellular accumulation or recycling of both ligand and/or metabolite. Quantitative analysis of each step is of critical importance to understand how to control tracer accumulation in ssr_2 expressing tumor cells. Thus, the objective of this study was to examine the effect of glycation on the internalization and recycling kinetics of radiolabelled octreotide and octreotate analogues.

Tyr³-octreotide (TOC), Tyr³-octreotate (TOCA) and their respective glucose- (Gluc), maltose- (Malt) and maltotriose- (Mtr) derivatives were synthesized via Fmoc-SPPS and subsequent carbohydrate conjugation. Radioiodination was performed using the iodogen method. Radiochemical yields ranged from 50 to 84 % after RP-HPLC-purification. Precursors for ^{99m}Tc-labelling (Gluc-Lys⁰(N-His)TOC (Gluc-K(H)-TOC) and Mtr-Lys⁰(N-His)TOC (Mtr-K(H)-TOC)) were prepared analogously to the peptides mentioned above. Labelling with ^{99m}Tc was carried out according to the $[[^{99m}\text{Tc}](\text{CO})_3(\text{H}_2\text{O})_3]^+$ aquaion protocol previously described [1]. For comparison, we also included [¹¹¹In]Octreoscan and [¹¹¹In]DOTATOC into our study.

Internalisation and externalisation experiments were performed using the ssr_2 expressing rat pancreatic tumor cell line AR42J. Free, surface bound and internalised radioactivity were determined after 10, 30, 60, 90 and 120 min. of incubation with the radioligands at 37°C. In the

externalisation experiments allowing ligand recycling, the fraction of radioactivity released into the supernatant during 10, 30, 60, 90 and 120 min as well as the radioactivity remaining in the cells were determined. We also measured the activity released during 5 subsequent incubations (10, 20 and 3x30 min) with intermediate changes of the medium (limited recycling).

The influence of carbohydratation of TOC on the internalization parallels the size of the sugar used. Compared to [^{125}I]TOC only the glucose conjugate showed enhanced uptake in the cells. In contrast, intracellular accumulation of both [^{125}I]Gluc-TOCA and [^{125}I]Mtr-TOCA (Fig.3 and Tab.2) was significantly increased (7.36 ± 0.50 and 5.68 ± 0.38 fold compared to [^{125}I]TOC). Comparing the internalisation characteristics of TOC and TOCA and of the respective glucosylated derivatives, we observed a synergistic effect of both structural modifications (substitution of Thr(ol)⁸ by Thr⁸ and carbohydratation) on surface availability and on internalisation rate. Compared to [^{111}In]Octreoscan and [^{111}In]DOTATOC, the internalization of both $^{99\text{m}}\text{Tc}$ -labelled carbohydrated derivatives was unexpectedly high.

Pretreatment experiments with $10\mu\text{M}$ sandostatin reduced the ligand uptake to a max. of 5% of control, indicating i) sst₂ specific uptake and ii) that no carbohydrate related uptake mechanism is involved (Tab.2). For all tracers investigated, the internalized activity strongly correlates with the surface availability of the ligands.

Table 2 Internalisation data obtained after a 60 min

incubation with AR42J cells Internalisation values as well as ratios are normalized to the reference [^{125}I]TOC

^a surface availability = % surface-bound ligand/% free radioligand

^b internalisation rate = % internalised ligand/% surface-bound ligand

* pre-treatment experiments with 10 M sandostatin reduced cellular ligand uptake by a minimum of 95%

	internalised ligand	surface availability	internalisation rate ^c
[^{125}I]Mtr-TOC	42 ± 7*	47 ± 11	87 ± 8
[^{125}I]Malt-TOC	66 ± 4	68 ± 11	95 ± 18
[^{125}I]TOC	100	100	100
[^{125}I]Gluc-TOC	143 ± 14	136 ± 13	110 ± 12
[^{125}I]TOCA	204 ± 7*	182 ± 6	140 ± 8
[^{125}I]Gluc-TOCA	736 ± 50*	583 ± 53	196 ± 21
[^{125}I]Mtr-TOCA	568 ± 38*	312 ± 25	216 ± 26
[^{111}In]Octreoscan	16 ± 2	24 ± 2	63 ± 12
[^{111}In]DOTATOC	30 ± 7	28 ± 7	55 ± 11
[$^{99\text{m}}\text{Tc}$]Gluc-K ⁰ (H)-TOC	234 ± 24	204 ± 54	171 ± 29
[$^{99\text{m}}\text{Tc}$]Mtr-K ⁰ (H)-TOC	298 ± 37	195 ± 35	186 ± 14

With respect to externalisation glycosylation seems to have no influence (Fig. 4). The degree of externalisation of radioligand from the cells is primarily determined by the nature of the peptide (TOC or TOCA) and also by the intracellular fate of the label. In the externalisation experiment that allowed ligand recycling, TOCA and its glycosylated derivatives showed about 2/3 of extracellularly located radioactivity compared to the experiment without recycling, while about 80% were found for TOC, Gluc-TOC and Mtr-TOC. [$^{99\text{m}}\text{Tc}$]Gluc-K⁰(H)-TOC as well as both ^{111}In -labelled compounds showed nearly quantitative retention in the cell within 120 min under recycling conditions. In contrast, intracellular activity of [^{111}In]Octreoscan and [^{111}In]DOTATOC was depleted by 33% and 49% during 120 min, when recycling was limited.

EXAMPLE 4**[Tc-99m] (CO)₃-Labeled Carbohydrated SSTR-ligands:****Synthesis, Internalization Kinetics and Biodistribution on a Rat Pancreatic Tumor Model.**

Aim: This study is to demonstrate the design of tracers for specific and high-level targeting of SSTR expressing tumors. For this purpose we introduced carbohydrate octreotide derivatives to optimize pharmacokinetics and to improve SSTR specific internalization and tumor retention. Here we describe compounds of a series of new carbohydrate ^{99m}Tc-SSTR ligands.

Methods: Coupling of glucose (Gluc) and maltotriose (Mtr) to N -Lys⁰ of N -(Boc-His(Boc))Lys⁰-Tyr³-Lys⁵(Dde) - octreotide (protected K(H)TOC) and final deprotection yielded Gluc- and Mtr-K(H)TOC. ^{99m}Tc-labeling was carried out using [^{99m}Tc(H₂O)₃(CO)₃]⁺. Internalization and externalization studies (<2h) were performed using the SSTR₂ expressing rat pancreatic cell line AR42J and [¹²⁵I]Tyr³-octreotide ([¹²⁵I]TOC) as a reference. Biodistribution was evaluated in nude mice bearing AR42J tumors at 0.5 and 2h p.i (n=4).

Results: Radiolabeling produced efficiently (0.5h, RCY>97%) uniform products. Compared to [¹²⁵I]TOC, both carbohydrate peptides showed significantly higher intercellular activity levels; e.g. at 2h 2.3±0.2 times higher levels for [^{99m}Tc]Gluc-K(H)TOC and 3.6±0.4 times higher levels for [^{99m}Tc]Mtr-K(H)TOC. Externalization studies revealed a decrease of about 50% of intracellular activity for [¹²⁵I]TOC within 2h, while the intercellular level of [^{99m}Tc]Gluc-K(H)TOC was almost stable up to 2h, demonstrating retention of this tracer. In vivo, tumor accumulation reached 12.2±1.0 and 14.0±6.3%ID/g at 2h p.i. with blood levels of 1.5±0.2%ID/g and 4.4±1.0%ID/g for

[^{99m}Tc]Gluc-K(H)TOC (T/liver 0.77, T/kidney 0.63) and [^{99m}Tc]Mtr-K(H)TOC (T/liver 0.97, T/kidney 0.84), respectively.

Conclusion: These results demonstrate the usefulness of carbonylation as a tool to improve SSTR targeting.

EXAMPLE 5

[Tc-99m] (CO)₃ -Labeled Carbonylated SSTR-ligands: Synthesis, Internalization Kinetics and Biodistribution on a Rat Pancreatic Tumor Model

Aim: This study is part of our endeavor to design tracers for specific and high-level targeting of SSTR expressing tumors. For this purpose we use suitable carbohydrate moieties to optimize the pharmacokinetics and to improve SSTR specific internalization and tumor retention. Here we describe for the first time carbonylated SSTR binding peptides labeled via the [^{99m}Tc(H₂O)₃(CO)₃]⁺ aquaion approach.

Methods: N (Boc-His(Boc))Lys⁰-Tyr³-Lys⁵(Dde)-octreotide (protected K(H)TOC) was synthesized using standard Fmoc-chemistry. Coupling of glucose (Gluc) and maltotriose (Mtr) to N -Lys⁰ and final deprotection yielded the Gluc- and Mtr-derivatives of K(H)TOC. Tc-99m-labeling was carried out using the organometallic aquaion [^{99m}Tc(H₂O)₃(CO)₃]⁺(1). Internalization and externalization studies (<120 min) were performed for both compounds using the SSTR₂ expressing cell line AR42J. For the in vitro studies [¹²⁵I]Tyr³-octreotide ([¹²⁵I]TOC) was used as a reference. Biodistribution of intravenously administered [^{99m}Tc]Gluc-K(H)TOC and [^{99m}Tc]Mtr-K(H)TOC was evaluated in nude mice bearing AR42J rat pancreatic tumors at 30 and 120 min p.i.(n=4).

Results: The labeling procedure produced efficiently (30 min, RCY>97%) uniform products (HPLC). Compared to the reference [¹²⁵I]TOC, both carbonylated peptides were significantly higher internalized at all time points

investigated; e.g. at 120 min 2.3 ± 0.2 times higher levels for [^{99m}Tc]Gluc-K(H)TOC and 3.6 ± 0.4 times higher levels for [^{99m}Tc]Gluc-K(H)TOC and 3.6 ± 0.4 times higher levels for [^{99m}Tc]Mtr-K(H)TOC. Furthermore, externalization studies revealed a decrease of about 50% of intracellular activity for the reference compound within 120 min, while the high level of intracellular [^{99m}Tc]Gluc-K(H)TOC was almost stable up to 2h, demonstrating retention of this tracer in the cell line investigated. In vivo, tumor accumulation reached 12.2 ± 1.0 and $14.0 \pm 6.3\%$ ID/g at 120 min p.i. with corresponding blood activity levels of $1.5 \pm 0.2\%$ ID/g and $4.4 \pm 1.0\%$ ID/g for [^{99m}Tc]Gluc-K(H)TOC (T/liver 0.77, T/kidney 0.63) and [^{99m}Tc]Mtr-K(H)TOC (T/liver 0.97, T/kidney 0.84), respectively.

Conclusion: These results demonstrate the usefulness of carbonylation as a tool to improve SSSTR targeting.

Example 6

Solid phase peptide synthesis

1. Fmoc-Lys⁰-Tyr³-Lys(Dde)⁵-octreotide (Fmoc-Lys⁰-TOC(Dde))
Fmoc-Thr(tBu)-ol

A solution of Fmoc-Thr(tBu)-OH (1.391 g, 3.5 mmol) in 30 ml of tetrahydrofuran (THF) was cooled to -10°C . N-methylmorpholine (386 μl , 3.5 mmol) and ethylchloroformate (333 μl , 3.5 mmol) were added successively. The reaction mixture was stirred at -10°C for 30 min. Then sodium borohydride (396 mg, 10.5 mmol) was added. Over a period of 30 min 60 ml of methanol were slowly added to the reaction mixture, which was then stirred at 0°C for 3 hours.

After the addition of 50-70 ml of 1 N HCl (the cloudy reaction mixture has to become transparent) the organic solvents were evaporated and the remaining aqueous phase

was extracted twice with dichloromethane (DCM). Extraction efficiency was monitored by thin layer chromatography (product $R_f=0.83$ in ethyl acetate (AcOEt)) of both phases. The combined organic layers were dried over magnesium sulfate, filtered and concentrated in vacuo to yield a yellowish oil. The crude product was purified by flash chromatography using AcOEt. The product was obtained as an oil (1.19g, 89%).

Calculated monoisotopic mass for $C_{23}H_{29}NO_4=383.21$; found: $m/z=406.1 [M=Na]^+$

SPPS of Fmoc-Lys⁰-Dphe¹-Cys²-Tyr³-DTrp⁴-Lys(Dde)⁵-Thr⁶-Cys⁷-Thr-ol⁸

DHP-HM (3,4-Dihydro-2H-Pyran-2-ylmethoxymethylpolystyrol)-resin (1.000 g, 0.94 mmol/g) was allowed to preswell in 10 ml of dry DCE (1,2-Dichloroethane) for 1 hour. Then a solution of Fmoc-Thr(tBu)-ol (1.266 g, 3.3 mmol) and of Pyridinium-p-toluenesulfonate (414 mg, 1.75 mmol) in 7 ml of dry DCE was added and the reaction mixture was stirred overnight at 80°C under argon. To cap free functional groups on the resin 5 ml of pyridine were added and the suspension was stirred for another 15 min at room temperature. The loaded resin was then filtered off, washed twice with DMF (N,N-Dimethylformamide) and with DCM and dried in an exsiccator. Final load of the resin was 0.834 mmol/g. The peptide sequence was assembled on the resin bound amino alcohol using standard Fmoc-protocol. Briefly, the N-terminal Fmoc was removed with 20% piperidine in DMF, and the resin of resin-supported peptide was washed with NMP (N-Methylpyrrolidone). Coupling was carried out in NMP by reacting 1.5 eq of amino acid derivative with 1.5 eq of HOBT(1-Hydroxybenzotriazol), 1.5 eq of TBTU (O-(1H-benzotriazol-1-yl)-N,N,N',N'-Tetramethyluronium-Tetrafluoroborate) and 3.5 eq of DIPEA (N-Ethyl-diisopropylamine). After adding the activated amino acid to the reaction vessel, the resin

was agitated for an appropriate amount of time (usually 40-60 min). The resin was then washed with additional NMP. The sequence of addition for the synthesis of TOC was Fmoc-Cys(Trt), Fmoc-Thr(tBu), Fmoc-Lys(Dde), Fmoc-DTrp, Fmoc-Tyr, Fmoc-Cys(Trt), Fmoc-Dphe and Fmoc-Lys(Boc). After the coupling of the last amino acid to the sequence, the resin was washed several times with NMP and DCM. Cleavage from the resin and deprotection of the Thr-, Cys- and Lys⁰-sidechains was performed using a mixture of TFA (trifluoroacetic acid)/TIBS (triisobutylsilane)/water (95:2.5:2.5) and DCM (1:1): After 90 min the resin was filtered and washed twice with DCM. The combined filtrates were concentrated using a rotary evaporator and the crude product was precipitated with ether. We obtained 828 mg of crude produce. Yield: 83%

The crude peptide was resuspended in 50 ml of THF (per 300 mg of peptide), and 5 mM ammonium acetate was added, until a clear solution was obtained. The pH was adjusted to 7 by dropwise addition of a saturated solution of NaHCO₃. Then 100 ul (per 300 mg of peptide) of hydrogen peroxide (30%) were added. After 30 min of stirring at room temperature cyclisation was complete (gradient HPLC-control: 30-80% B in 15 min). The solvents were evaporated, and the cyclised product was lyophilized. Yields were quantitative.

Calculated monoisotopic mass for C₈₀H₁₀₀N₁₂O₁₆S₂=1548.68;
found: m/z =1549.5 [M+H]⁺, m/z =1571.5 [M+Na]⁺

2. Fmoc-Lys⁰-Tyr³-Lys(Dde)⁵-octreotide (Fmoc-Lys⁰-TATE(Dde))
Fmoc-Lys⁰-Dphe¹-Cys²-Tyr³-DTrp⁴-Lys(Dde)⁵-Thr⁶-Cys⁷-Thr⁸
To 1.502 g of dry TCP-resin a solution of 894 mg (2.25 mmol) of Fmoc-Thr(tBu) and 321 ul (1.87 mmol) of DIPEA in 15 ml of dry DCM was added. After stirring for 5 min,

another 642 μ l (3.76 mmol) of DIPEA were added. After vigorous stirring for 90 min at room temperature, 1.5 ml of methanol were added to cap unreacted Tritylchloride groups. After 15 min the resin was filtered, washed twice with DCM, DMF and methanol respectively and dried *in vacuo*. Final load of the resin was 0.77 mmol/g. Synthesis of the peptide sequence Cys(Trt)-Thr(tBu)-Lys(Dde)-DTrp-Tyr-Cys(Trt)-Dphe-Lys(Boc)-Fmoc on the resin-bound amino acid, deprotection and cleavage from the resin as well as cyclisation were performed as described for Fmoc-Lys⁰-TOC(Dde).

Calculated monoisotopic mass for C₈₀H₉₈N₁₂O₁₇S₂=1562.66;
found: m/z = ([M+H]⁺)

Solution phase derivatization

1. Lys⁰(N_ε-Boc-His(Boc))-TOC(Dde)

A solution of 500 mg (0.32 mmol) of Fmoc-Lys⁰-TOC(Dde), 170 mg (0.48 mmol) of Boc-His(Boc), 65 mg (0.048 mmol) of HOBt, 154 mg (0.48 mmol) of TBTU and 300 μ l (1.75 mmol) of DIPEA in 3 ml of DMF was stirred at room temperature. RP-HPLC analysis (gradient: 30-80% B in 15 min) revealed that the reaction was complete within 30 min. The product was precipitated using water and dried *in vacuo*. To remove the N-terminal Fmoc-protecting group, the peptide was dissolved in 1 ml piperidine/DMF (1:4) and stirred for 15 min. Precipitation with ether afforded the deprotected product with a yield of 86%.

Calculated monoisotopic mass for C₈₁H₁₁₃N₁₅O₁₉S₂=1663.78;
found: m/z=1873.6 [M+H]⁺, m/z=1895.7 [M+Na]⁺

2. Lys⁰-N⁰-Amadori derivatives of Lys⁰(Boc-His(Boc))-TOC(Dde)

Based on a method reported previously¹, 1 equiv. of Lys⁰-(Boc-His(Boc))-TOC(Dde) and 10 equiv. of the respective aldose (Glucose=S1, Maltose = S2, Maltotriose = S3) were dissolved in methanol/acetic acid (95:5), and the reaction mixture was stirred at 60°C for 24-48 h. The solvents were then evaporated, and the crude product was precipitated by the addition of ether.

To remove the Dde-protection group, the glycosylated peptide was redissolved in a small volume of DMF, 2 vol % of hydrazine hydrate were added and the solution was stirred at room temperature for 15 min. The deprotected peptide was precipitated by the addition of ether, washed with ether and dried in vacuo. Boc-protecting groups on the His-residue were then removed redissolving the crude products in a small volume of TFA/TIBS/water (95:2.5:2.5) and stirring for 15 min at room temperature. The products were precipitated using ether and purified via preparative RP-HPLC (gradient: 10-60% B in 30 min). Yields ranged from 17-32%.

S1-Lys⁰(His)TOC(N_α-(1-deoxy-D-fructosyl)-Lys⁰N_ε-His)-Tyr³-octreotide):

Calculated monoisotopic mass for C₆₇H₉₅N₁₅O₁₈S₂=1461.60;

found: m/s = 1873.6 [M+H]⁺, m/z = 1895.7 [M+Na]⁺

S2 Lys⁰(His)TOC(N_ε-(O-β-D-glucopyranosyl-(1-4)-1-deoxy-D-fructosyl)-Lys⁰(N_ε-His)-Tyr³-octreotide):

Calculated monoisotopic mass for C₇₃H₁₀₅N₁₅O₂₃S₂=1623.70;

found: m/z = 1873.6 [M+H]⁺, m/z = 1895.7 [M+Na]⁺

S3 Lys⁰(His)TOC(N_α-(O-α-D-glucopyranosyl-(1-4)-O-β-D-glucopyranosyl-(1-4)-1-deoxy-D-fructosyl)-Lys⁰(N_ε-His)-Tyr³-octreotide):

Calculated monoisotopic-mass for $C_{79}H_{115}N_{15}O^{28}S^2 = 1785.75$;
found: $m/z = 1873.6$ $[M+H]^+$, $m/z = 1895.7$ $[M+Na]^+$

3. Lys0 (N -2-picolylamino-...)TATE (Dde)

2-Picolylamine N,N-diacetic acid²

Imino diacetic acid (3.25 g, 24.4 mmol) was dissolved in a mixture of 30 ml of absolute ethanol and a solution of 1.95 g of NaOH (49 mmol) in 10 ml of water. After the addition of 4.00 g of picolylchloride (24.4 mmol) in 9 ml of water and of 1.95 g of NaOH (49 mmol) in 4 ml of water, the solution was stirred at 70°C for 2 h. Then another 1.95 g (49 mmol) of NaOH were added and the solution was stirred for another 1.5 h at 70°C. TLC reaction control (AcOEt) revealed complete disappearance of the reactants at that time. The solvents were evaporated in vacuo, and the residue was redissolved in 25 ml of water. After adjusting the pH of the solution to 1.5 with concentrated hydrochloric acid, the solution was again evaporated to dryness. By several successive steps of resuspension of the residue with methanol under reflux, hot filtration of the suspension and concentration of the filtrate in vacuo, excess NaCl was successfully removed. The picolylamino diacetic acid crystallized from the remaining methanolic solution overnight at -20°C.

Calculated monoisotopic mass for $C_{10}H_{12}N_2O_4 = 224.08$;
found: $m/z = [M+H]^+$ (disodium salt)

Coupling of 2-picolylamine N,N-diacetic acid to Fmoc-Lys⁰-TATE (Dde)

A solution of 52 mg (0.19 mmol) of 2-picolylamine N,N-diacetic acid, 26 mg (0.19 mmol) of HOBT, 62 mg (0.19 mmol) of TBTU and 176 μ l (1.75 mmol) of DIPEA in 2 ml of DMF was stirred at room temperature for 10 min. This solution was added dropwise to a solution of 200 mg (0.13

mmol) of Fmoc-Lys⁰-TATE(Dde) in 1 ml of DMF under vigorous stirring. After 30 min the product was precipitated using diethyl ether and dried *in vacuo*. To remove the N-terminal Fmoc-protecting group, the peptide was dissolved in 2 ml piperidine/DMF (1:4) and stirred for 10 min. Precipitation with ether afforded the deprotected product with a yield of 84%.

Calculated monoisotopic mass for C₇₅H₉₈N₁₄O₁₆S₂ = 1546.66;
found: m/z = [M+H]⁺, m/z = [M+Na]⁺

4. Lys⁰-N_a-Amadori derivatives of Lys⁰ (Pic)TATE(Dde)

Conjugation of Lys⁰(Pic)TATE(Dde) with glucose and subsequent Dde-deprotection were carried out as described for the Lys⁰-N_a-Amadori derivatives of Lys⁰(Boc-His(Boc))-TOC(Dde).

Calculated monoisotopic mass for C₇₁H₉₆N₁₄O₂₁S₂ = 1544.63;

found: m/z = [M+H]⁺, m/z = [M+Na]⁺

Radiolabelling

Based on the organometallic aquation [^{99m}Tc(H₂O)₃(CO)₃]⁺-method reported recently³, 10 mg of NaBH₄, 8 mg of Na₂CO₃ and 41.5 mg of Na/K tartrate were dissolved in 600 µl of [^{99m}Tc]pertechnetate eluate in a glass flask. The flask was then connected to a CO-filled balloon and sealed tightly. After stirring at 75°C for 45 min, the solution was cooled on an ice bath and 150 µl of phosphate buffered saline (PBS, pH-7.4) were added. To destroy the reducing agent, 600 µl of 1 N HCl were added. Then the solution was neutralized with 500 µl

of a saturated solution of NaHCO_3 . The presence of the $[\text{}^{99\text{m}}\text{Tc}(\text{H}_2\text{O})_3(\text{CO})_3]^+$ -aquaion was confirmed via TLC (5% conc. HCl in methanol).

After adding 1 ml of the $[\text{}^{99\text{m}}\text{Tc}(\text{H}_2\text{O})_3(\text{CO})_3]^+$ -solution (51 MBq) to 700 μg of $\text{S1-Lys}^0(\text{His})\text{TOC}$, the mixture was heated to 75°C for 30 min. Gradient HPLC purification afforded the radiochemically pure peptide $\text{Na}-(1\text{-deoxy-D-fructosyl})\text{-Lys}^0(\text{N-His}[\text{}^{99\text{m}}\text{Tc}(\text{H}_2\text{O})_3(\text{CO})_3]^+)-\text{Tyr}^3\text{-octreotide}$ with a radiochemical yield of 34%.

$\text{S3-Lys}^0(\text{His})\text{TOC}$ was labelled in an analogous manner.

Determination of Lipophilicity

To a solution of app. 300000 cpm of radiolabeled peptide in 500 ml of PBS (pH 7.4), 500 ml of octanol were added ($n=6$). Vials were vortexed for 3 min and then centrifuged at 15000 rpm for 6 min. Aliquots of 100 ml of PBS and octanol were measured in a γ -Counter.

$\text{S1-Lys}^0(\text{His})\text{TOC}$: $\log \text{Pow} = -0.673 \pm 0.064$

$\text{S3-Lys}^0(\text{His})\text{TOC}$: $\log \text{Pow} = -1.304 \pm 0.040$

In vitro experiments

AR42J cells were maintained in RPMI 1640, supplemented with 10% FCS and 2 mM L-glutamine.

Internalization studies

Six-well-plates with a cell population of $8 \times 10^5 - 5 \times 10^6$ AR42J-cells per well were incubated at 37°C with fresh culture medium (RPMI 1640, 1% BSA, 2 mM L-glutamine) for 1 h prior to the experiment. Then app. 300000 cpm of radiometallated peptide in 10 μl of culture medium were added to each well (triplicate experiments for the reference compound (internal standard) $[\text{}^{125}\text{I}]\text{TOC}$ and for the radiometallated compound of interest each). After

incubating for 10, 30, 60, 90 or 120 min. At 37°C the supernatant was collected and the cells were washed once with 1 ml of cold medium. The supernatant was pooled with the supernatant of the previous step. To remove receptor bound (acid releasable) radioactivity the cells were incubated at 37°C with 1 ml of 0,02 M NaOAc (acid wash). After 10 min. The supernatant was collected, the cells were washed once with 1 ml of 0,02 M NaOAc and the supernatant was again pooled with the supernatant of the previous step. Then the cells were extracted with 1 ml of 1 N NaOH and the wells were rinsed once with PBS. This pooled fraction represents internalized radioligand. The activity in the NaOH-fraction as well as in the supernatant- and in the acid wash-fractions was counted in a γ -Counter.

Externalization studies

As described for the internalization studies, the six-well-plates were incubated at 37°C with fresh culture medium (RPMI 1640, 1% BSA, 2 mM L-Glutamine) for 1 H prior to the experiment. Then app. 300000 cpm of radiometallated peptide in 10 μ l of culture medium were added to each well (triplicate experiments for the reference compound (internal standard) [125 I]TOC and for the radiometallated compound of interest each). After incubating for 120 min. At 37°C, the supernatant was collected and the cells were washed once with 1 ml of cold medium. The supernatant was pooled with the supernatant of the previous step. To collect externalized radioactivity the cells were then incubated at 37°C with 1 ml of culture medium. After 10, 30, 60, 90 and 120 min. Respectively the supernatant was collected, the cells were washed once with 1 ml of culture medium and the supernatant was again pooled with the supernatant of the previous step. Then the cells were

extracted with 1 ml of 1 N NaOH and the wells were rinsed once with PBS. This pooled fraction represents radioligand still located in the cell. The activity in the NaOH-fraction as well as in the supernatant-and in the externalisation-fractions was counted in a γ -Counter.

Externalization studies without recycling of the tracer

As described for the previous experiment, a six-well plate was incubated for 120 min. At 37°C with radioligand. The supernatant was collected and the cells were washed once with 1 ml of cold medium. The supernatant was pooled with the supernatant of the previous step. To collect externalized radioactivity the cells were then incubated at 37°C with 1 ml of culture medium. After 10 min. The supernatant was collected and the cells were again incubated with 1 ml of culture medium for another 20 min. At 37°C. The supernatant was collected and the cells were three more times incubated with 1 ml of culture medium for 30 min. At 37°C. Then the cells were extracted with 1 ml of 1 N NaOH and the wells were rinsed once with PBS. This pooled fraction represents radioligand still located in the cell. The activity in the NaOH-fraction as well as in the externalisation-fractions at all time points was counted in a γ -Counter.

Biodistribution studies

To establish tumor growth, subconfluent monolayer cells were treated with 1mM EDTA, suspended, centrifuged and resuspended in RPMI 1640.

Nude mice (male and female, 6-8 weeks) were inoculated s.c. in the flank with $2.5-3 \times 10^7$ cells suspended in 100 μ l of PBS (pH 7.4), were injected i.v. into the tail vein of nude mice bearing an AR42J tumor. The animals (n=3-4 were

sacrificed 30 and 120 min p.i., and the organs of interest were dissected. The radioactivity was measured in weighted tissue samples using a gamma counter. Data are expressed in % iD/g tissue (mean $\pm$ DS, n=3-4).

Table 1

Tissue accumulation [%iD/g]
Of [99m Tc]S1-Lys⁰(His)TOC
And [99m Tc]S3-Lys⁰(His)TOC
In AR42J tumor bearing
Nude mice 2 h p.i. (n=3-4)

	[99m Tc]S1-Lys ⁰ (His)TOC	[99m Tc]S3-Lys ⁰ (His)TOC
blood	1.49 $\pm$ 0.18	4.12 $\pm$ 0.87
liver	15.89 $\pm$ 2.70	14.34 $\pm$ 1.55
intestine	2.83 $\pm$ 0.28	2.02 $\pm$ 0.41
stomach	11.28 $\pm$ 2.74	6.22 $\pm$ 0.75
kidney	19.49 $\pm$ 2.22	17.97 $\pm$ 2.76
muscle	0.22 $\pm$ 0.04	0.40 $\pm$ 0.10
adrenals	6.47 $\pm$ 1.46	4.94 $\pm$ 0.38
pancreas	6.43 $\pm$ 2.09	3.32 $\pm$ 0.38
tumor	12.21 $\pm$ 0.96	14.02 $\pm$ 6.33

5 The discussion of documents, acts, materials, devices, articles and the like is included in this specification solely for the purpose of providing a context for the present invention. It is not suggested or represented that any or all of these matters formed part of the prior art base or were common general knowledge in the field relevant to the present invention as it existed before the priority date of each claim of this application.

10 Throughout the description and the claims of this specification the word "comprise" and variations of the word, such as "comprising" and "comprises" is not intended to exclude other additives, components, integers or steps.

THE CLAIMS DEFINING THE INVENTION ARE AS FOLLOWS:

1. A somatostatin receptor (sst) binding molecule comprising:
a ligand comprising natural or unnatural amino acids or a
5 peptidomimetic structure;
at least one multifunctional linker unit;
a carbohydrate; and
a chelating group allowing mono- or multidentate complexation
of a radioisotope selected from Tc and Re.
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2. The molecule of claim 1, wherein the radioisotope is an
isotope of Tc.
3. The molecule of claim 1, wherein the chelating group is
15 bound to the N-terminal of the ligand and the carbohydrate is
bound to the chelating group.
4. The molecule of claim 1, wherein the carbohydrate is bound
to the N-terminal of the ligand and the chelating group is
20 bound to the carbohydrate.
5. The molecule of claim 1, wherein the carbohydrate is a
sugar.
- 25 6. The molecule of claim 5, wherein the sugar is a mono- or
polysaccharide.
7. The molecule of claim 1, wherein the carbohydrate is
coupled to the ligand, to the multifunctional linker unit, or
30 to the chelator via a glycosidic bond.
8. The molecule of claim 1, wherein the carbohydrate is a
coupling product between an amino group of the ligand, the
multifunctional linker unit, or the chelator, and an aldose via
35 Amadori Reaction.

9. The molecule of claim 1, wherein the carbohydrate is a sugar selected from the group consisting of glucose, maltose, and maltotriose.

5 10. The molecule of claim 1, wherein the ligand is glycosylated at the N-terminal.

11. The molecule of claim 1, wherein the multifunctional linker unit is bound to the C-terminal of the ligand, and the
10 carbohydrate and the chelating group are bound to the multifunctional linker unit.

12. The molecule of claim 1, wherein the multifunctional linker unit is bound to the N-terminal of the ligand, and the
15 carbohydrate and the chelating group are bound to the multifunctional linker unit.

13. The molecule of claim 1, wherein the multifunctional linker unit is bound to the N-terminal of the ligand, the
20 chelating group is bound to the multifunctional linker unit, and the carbohydrate is bound to the chelating group.

14. The molecule of claim 1, comprising at least two ligands.

25 15. The molecule of claim 14, wherein the two ligands are bound to the multifunctional linker unit, and both the chelating group and the carbohydrate are bound to the multifunctional linker.

30 16. The molecule of claim 14, comprising at least two carbohydrates, each bound to the N-terminal of a ligand, wherein said carbohydrates are bound to a multifunctional linker unit, and the chelating group is bound to the multifunctional linker unit.

17. The molecule of claim 14, comprising at least two multifunctional linker units and at least two carbohydrates, wherein each carbohydrate is bound to a multifunctional linker unit, each multifunctional linker unit is bound to the N-terminal of a ligand, and each multifunctional linker unit is bound to the chelating group.

18. The molecule of claim 14, wherein the ligands are bound to the multifunctional linker unit, the chelating group is bound to the multifunctional linker unit, and the carbohydrate is bound to the chelating group.

19. The molecule of claim 14, wherein the carbohydrate is a sugar, and the sugar is a coupling product between an amino group of the ligand, the multifunctional linker unit, or the chelator, and an aldose via Amadori Reaction.

20. The molecule of claim 14, wherein the carbohydrate is coupled to the ligand, to the multifunctional linker unit, or to the chelator via a glycosidic bond.

21. A pharmaceutical composition comprising the molecule of any one of claims 1 to 20 and a pharmaceutically acceptable carrier.

22. A method of imaging selected from the group consisting of sst-imaging which comprises administering to a patient the composition of claim 21.

23. The compound $[^{99m}\text{Tc}]\text{Gluc-K}^0(\text{H})\text{TOC}$.

24. The compound $[^{99m}\text{Tc}]\text{Mtr-K}^0(\text{H})\text{TOC}$.

25. The compound $[^{99m}\text{Tc}]\text{Gluc-K}^0(\text{H})\text{TOCA}$.

26. The molecule of claim 1 or claim 14, wherein the chelating group is selected from the group consisting of histidine, picolylamine diacetic acid, hydroxy nicotine amide (HYNIC), mercaptoacetyl-glycyl-glycyl-glycine (MAG3), and tetrapeptides.

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27. The molecule of claim 1, substantially as hereinbefore described with reference to any one of the Examples and/or Figures.

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FIGURE 1A

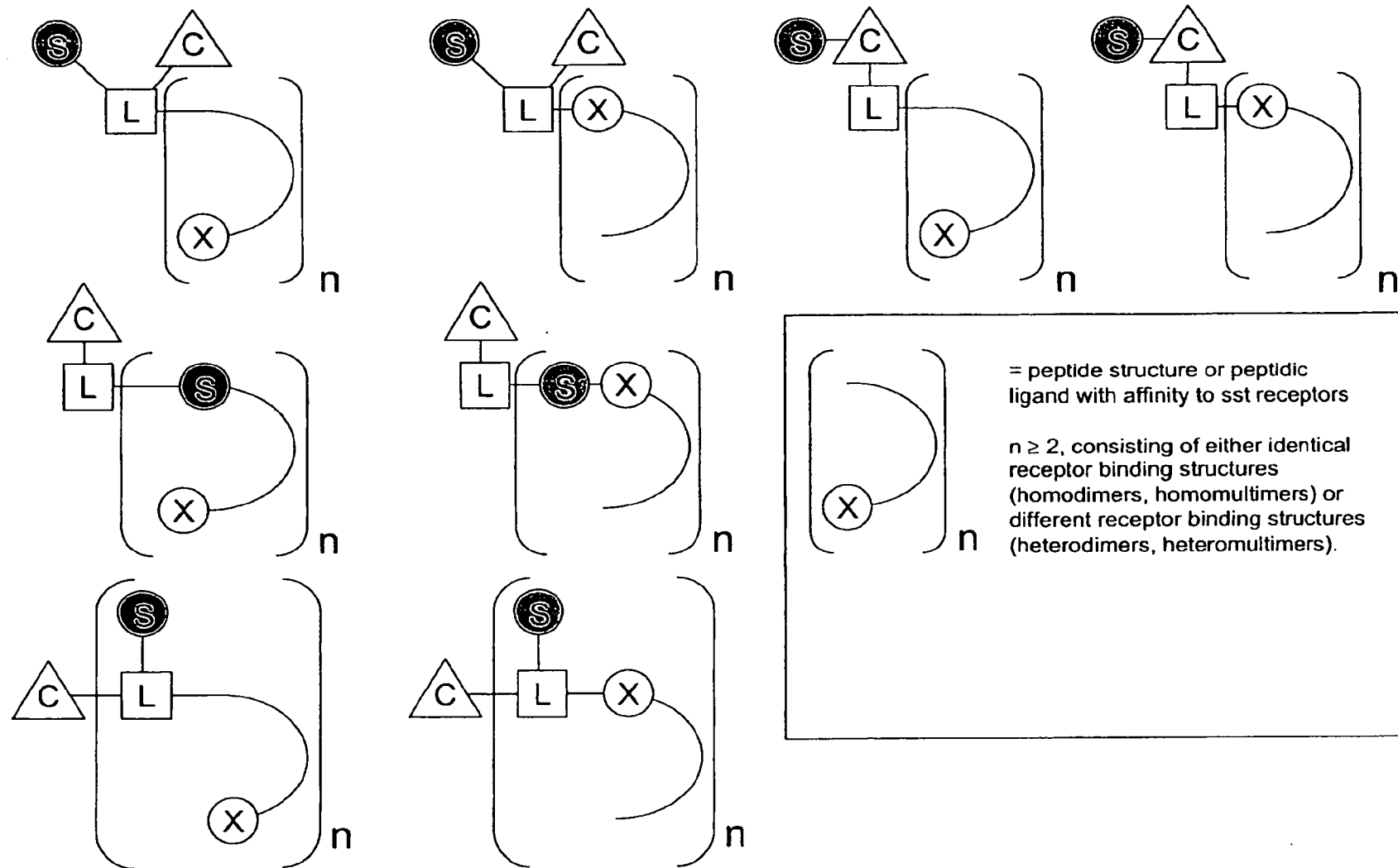


FIGURE 1B

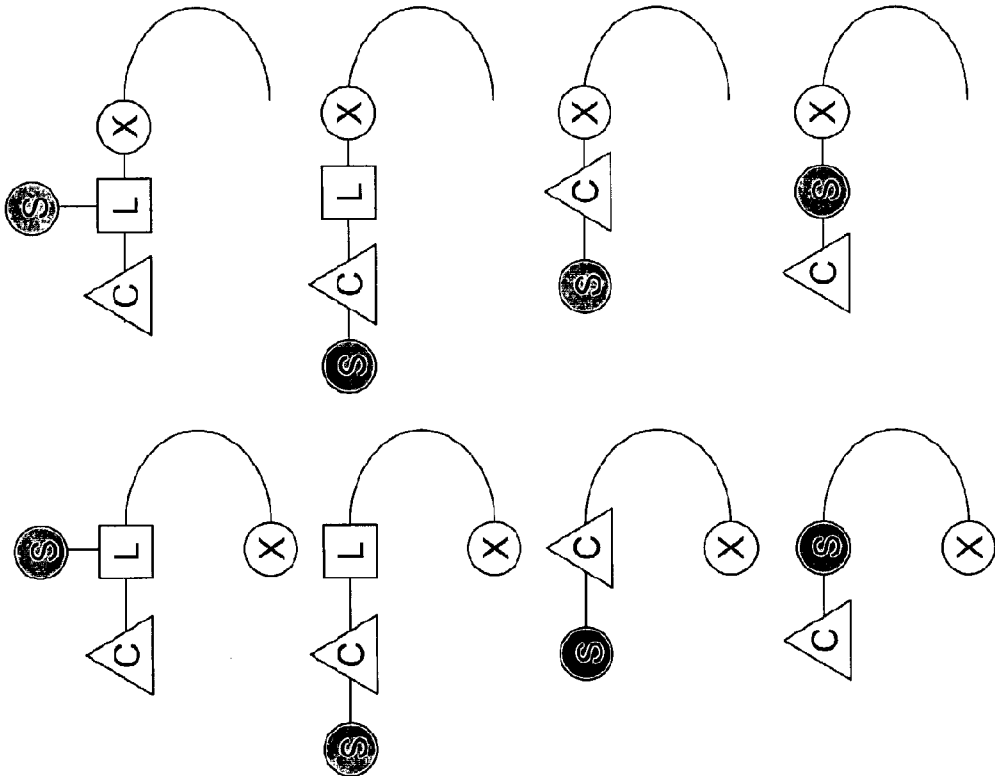


FIGURE 1C

