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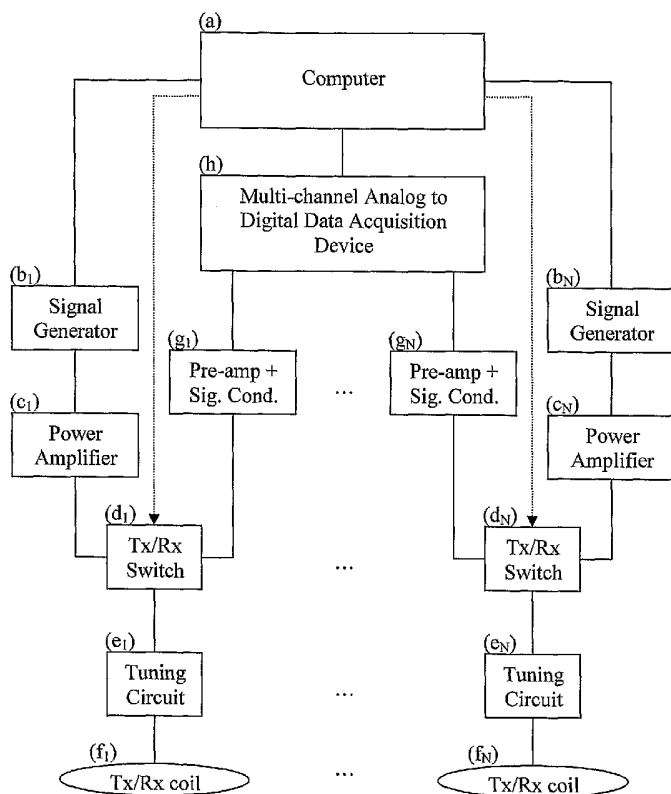
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- (71) Applicant and (72) Inventor: WALSH, David, O. [US/US]; 8849 47th Place W., Mukilteo, WA 98275-3467 (US).
- (74) Agents: EVANS, Stephen, M. et al.; Graybeal Jackson Haley LLP, 155 - 108th Ave NE, Suite 350, Bellevue, WA 98004-5973 (US).
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(54) Title: MULTICOIL NMR DATA ACQUISITION AND PROCESSING METHODS



(57) Abstract: A multicoil NMR data acquisition apparatus and processing method for performing three-dimensional magnetic resonance imaging in a static magnetic field without the application of controlled static magnetic field gradients. A preferred application relates specifically to the detection and localization of groundwater using the Earth's magnetic field. Multicoil arrays are used in both transmit and receive modes, and coherent data processing algorithms applied to the data to generate three-dimensional NMR spin density estimates. Disclosed are methods for acquiring NMR data using an array of at least two transmit and receive coils, and for processing such multicoil data to estimate the three-dimensional NMR spin density distributions.

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MULTICOIL NMR DATA ACQUISITION AND PROCESSING METHODS

Benefit of provisional application No. 60/485,689, filed on 9 July 9 2003, is claimed.

5

BACKGROUND OF THE INVENTION

Multicoil MRI has been used for many years to non-invasively examine the nuclear magnetic resonance (NMR) spin density distribution within three dimensional objects or
10 volumes. Typically, using existing MRI data acquisition methods and data processing methods, the object under investigation is placed in a static magnetic field B_0 and is energized by an alternating magnetic field B_1 . The frequency of the alternating magnetic field B_1 is selected as the Larmor frequency (the natural nuclear magnetic resonant frequency) for the atomic species of interest. The Larmor frequency depends upon the magnitude of the static
15 field B_0 , among other factors. A number of well-known MRI applications have detected the hydrogen proton spin density, although it is possible to image carbon, potassium and other atomic species with certain nuclear spin properties.

Typically, using existing MRI data acquisition methods and data processing methods, magnetic field gradients are applied across the object under investigation, either during or after
20 the application of the alternating field B_1 . These magnetic field gradients cause the frequency of the NMR signal to vary in a predictable way along the various spatial dimensions of the object under investigation. Thus, in the prior state of the art of MRI, spatial localization is accomplished by frequency and/or phase encoding of the object through the application of controlled magnetic field gradients.

25 Some existing MRI devices are designed to use multiple coils during data acquisition, and some conventional MRI data processing methods exploit the differences between the individual coil fields to enhance the spatial resolution and quality of the NMR image. See for example United States patent no. 6,160,398. However, all existing MRI devices, MRI data acquisition methods and MRI data processing methods derive some or all of the spatial
30 information required for imaging in three dimensions through the application of magnetic gradient fields.

While existing MRI devices, data acquisition methods and data processing methods may be suitable for the particular purpose to which they address, they are not as suitable for performing three dimensional magnetic resonance imaging in a static magnetic field without the application of controlled static magnetic field gradients.

5 A primary limitation of existing MRI devices and methods is the requirement to generate and control gradients in the static field B_0 . The generation and control of such gradients requires specially designed gradient field coils, and these coils are typically only effective when employed in certain constrained geometries. For example, in medical MRI, a great deal of research has been undertaken to design and construct the gradient coils for
10 specific MRI scanner designs, and the gradient coil assemblies represent a significant portion of the scanner's expense. Most conventional MRI scanners use gradient coils that surround the object under investigation in order to produce approximately linear field gradients.

For many potential applications of three-dimensional MRI, the requirement to generate and control static field gradients is either impractical or prohibitively expensive. For example,
15 in the investigation of subsurface groundwater distributions via surface coil NMR measurements, the generation of significant gradients in the Earth's magnetic field at operationally significant depths would require large amounts of power and complex arrays of magnetic field antennae. The imaging of other large fixed objects, such as bridge supports and building foundations, is similarly constrained by power requirements and the difficulty in
20 generating and controlling static field gradients in three dimensions. Other potential applications of MRI, such as industrial non-destructive evaluation of raw materials, are not presently commercially viable due to the expense and geometrical constraints associated with conventional gradient-based MRI scanners.

Surface NMR data acquisition methods and data processing methods have been used for
25 many years to detect and localize subsurface groundwater. The existing state of the art in surface NMR utilizes a single surface coil to generate the alternating B_1 field. The B_1 field is transmitted with various levels of energy, and the measured NMR signals received on the same coil or a single separate coil are mathematically processed to estimate a profile for the groundwater distribution in one dimension only: depth. While existing surface NMR devices,
30 data acquisition methods and data processing methods may be suitable for the particular purpose to which they address, they are not as suitable for performing three dimensional magnetic resonance imaging in a static magnetic field without the application of controlled

static magnetic field gradients. The present state of the art in surface NMR techniques can produce, at best, an estimate of the 1-dimensional groundwater density profile directly beneath the coil. These 1-D profile estimates are subject to a variety of errors stemming from the use of a single surface coil, and inaccurate 1-D models of the coil fields and water density profiles.

5 Presently available 1-D profile estimation techniques, which are based on single coil surface NMR systems, rely on a single measurement variable: the transmitted pulse energy and its relation to tip angle, to estimate a water density profile in depth. The NMR signal amplitude at a given point in space is a sinusoidal function of the flip angle at that location. Present 1-D inversion techniques measure the NMR signal using different transmit pulse energy levels, and
10 then fit the set of NMR amplitudes to a simplified 1-D model. To make the inversion tractable, the coil vector field lines are assumed to be parallel and confined to a cylinder directly beneath the coil, and the water density profile is assumed to vary in one dimension only.

**Reliance on one dimensional modeling according to the prior art therefore engenders certain deficiencies. A first fundamental problem is that the coil field lines are
15 very different from the assumed cylindrical model over large portions of the investigation space. The generated signal depends upon the angle between the earth's vector field and the coil's vector field. A second fundamental problem is the assumption that the water density profile varies in one dimension only. Three-dimensionally variant aquifers, which are common in nature, cannot be adequately characterized using simple 1-D models. A
20 third fundamental problem is that even if accurate coil field models were employed and 3-D water distributions were allowed, the resulting inversion would suffer from ambiguities. The integrated NMR signal depends on the 3-D distribution of water, the coil field lines, the Earth's field direction, and the transmitted pulse energy. Varying the pulse energy alone does not provide enough information to unambiguously solve the 3-D
25 inversion problem.**

SUMMARY OF THE INVENTION

In view of the foregoing deficiencies inherent in the known types of multicoil NMR
30 data acquisition methods and data processing methods now present in the prior art, the present invention provides new multicoil NMR data acquisition and processing methods wherein the

same can be utilized for performing three dimensional magnetic resonance imaging in a static magnetic field without the application of controlled static magnetic field gradients.

The general purpose of the present invention, which will be described subsequently in greater detail, is to provide a new multicoil NMR data acquisition and processing method that has many of the advantages of the multicoil NMR data acquisition methods and data processing methods mentioned heretofore and many novel features that result in a new multicoil NMR data acquisition and processing method which is not anticipated, rendered obvious, suggested, or implied by any of the prior art multicoil NMR data acquisition methods and data processing methods, either alone or in any combination thereof.

To attain this, an embodiment of the present invention generally comprises a method for acquiring NMR data using an array of two or more transmit coils and two or more receive coils, and a method for processing such multicoil data to estimate the three-dimensional NMR spin density distribution within the object or volume under investigation. Features of the embodiment include a multicoil NMR data acquisition method, which utilizes multiple coil arrays in both transmit mode and receive mode, and which does not involve the generation or control of gradients in the static magnetic field; a method for processing the data acquired via the multicoil NMR data acquisition method, which yields a three-dimensional estimate of the NMR spin density distribution.

The multicoil NMR data acquisition method uses an array of at least two transmit coils, and at least two receive coils. A single multi-coil FID measurement is recorded by driving the transmit coils with a current pulse at the Larmor frequency of the target, and after a short delay, recording the resulting NMR free induction decay signal for each of the receive coils. A series of independent measurements are obtained by using unique combinations of relative amplitudes and/or phases on the transmit coils, and unique total transmitted energy levels. The use of multi-coil arrays in both the transmit and receive modes introduces a unique dependence between the acquired set of signals generated by an isolated point source in space and the vector fields of the various coils relative to that point in space. The variance among the vector coil fields over the three-dimensional imaging volume makes it possible to isolate and locate signal sources in three dimensions.

The data processing method embodiment comprises specific data processing methods for processing NMR data acquired via the multicoil NMR data acquisition arrangement: a matched filtering data processing method, an adaptive filtering data processing method, and a

linear inverse/least-squares data processing method. These data processing methods yield three-dimensional estimates of the NMR spin density distribution of the target. The data processing methods also yield estimates of the time-domain NMR signal processes emanating from discrete locations in the volume. These time-domain signal estimates can be further
5 processed using previously developed analysis techniques to yield additional information on the physical properties of the materials under investigation.

The invention is not limited in its application to the details of construction and to the arrangements of the components set forth in the following description or illustrated in the drawings. The invention is capable of other embodiments and of being practiced and carried
10 out in various ways. Also, it is to be understood that the phraseology and terminology employed herein are for the purpose of the description and should not be regarded as limiting.

BRIEF DESCRIPTION OF THE DRAWINGS

15 Various other objects, features and attendant advantages of the present invention will become fully appreciated as the same becomes better understood when considered in conjunction with the accompanying drawings, in which like reference characters designate the same or similar parts throughout the several views, and wherein:

20 FIG.1 is a block diagram of a multi-channel NMR data acquisition apparatus that uses separate coils for transmit and receive functions.

FIG.2 is a block diagram of a multi-channel NMR data acquisition apparatus that uses the same array of coils for transmit and receive functions.

25

DETAILED DESCRIPTION OF THE INVENTION

Multicoil NMR Data Acquisition Procedure:

An array of at least two transmit coils and at least two receive coils are arranged in the
30 vicinity of the object or volume to be investigated. A single NMR measurement is performed by driving one or more of the transmit coils with an alternating current at the Larmor (resonant) frequency of the target, e.g., water, and then recording the resulting NMR signal from the at

least two receive coils. A series of such NMR measurements are performed using at least two linearly independent combinations of relative current amplitudes and/or phases among the transmit coils (henceforth referred to as the transmit array combination), and using at least two values of total transmitted energy for each transmit array combination.

5

Detailed description of a single data acquisition method:

Turning now descriptively to the drawings, FIG. 1 illustrates a functional apparatus for acquiring multicoil NMR data according to an embodiment of the present invention, which
10 comprises a method for acquiring surface NMR data using an array of at least two transmit and receive coils and a method for processing such multicoil data to estimate the three-dimensional NMR spin density distribution within the object or volume under investigation.

FIGURE. 1 depicts the generic hardware systems and processes involved in the
15 multicoil data acquisition procedure. The data acquisition process is controlled by computer (a). The computer (a) in concert with signal generator(s) ($b_1 - b_N$), produces a transient waveform(s), or pulse(s), on the selected transmit coil(s). The waveform for each transmit pulse(s) is amplified to the desired level by a power amplifier(s) ($c_1 - c_N$). The amplified current pulse(s) drives a tuning circuit(s) ($d_1 - d_N$) and transmit coil(s) ($e_1 - e_N$). The amplified
20 current in the transmit coil(s) produces the B1 field, and the B1 field causes the nuclear magnetic moments of susceptible molecules to precess about the B0 field in phase with the B1 field. During the application of the transmit pulse(s), the receive Tx/Rx switches ($h_1 - h_N$) are left open to prevent damage to sensitive electronic components in the receive chain. The receive tuning circuits ($g_1 - g_N$) may be set to a low-Q state during and/or slightly after the
25 application of the transmit pulse, to rapidly dissipate transient currents in the receive coils caused by the large amplitude B1 fields.

After the termination of the transmit pulse(s), and a short additional time delay to allow transient currents to decay, the Tx/Rx switches ($h_1 - h_N$) are closed and signal acquisition is initiated. If the tuning circuits ($g_1 - g_N$) were set to a low-Q state during the transmit operation,
30 they may be retuned to a high-Q to optimize reception of the weak narrowband NMR signal during receive mode. The precessing magnetic moments generate alternating magnetic fields, which in turn generate currents on the receive coils ($f_1 - f_N$). The received current sources are

routed through the tuning circuits ($g_1 - g_N$) and Tx/Rx switches ($h_1 - h_N$) and amplified by pre-amplifiers ($i_1 - i_N$) and filtered by signal conditioning circuits ($i_1 - i_N$). The amplified and conditioned analog voltages or currents are sampled and converted to digital signals by a multi-channel analog to digital (A/D) data acquisition device (j). The A/D device (j) is controlled by the computer (a). Digital signals from the A/D device (j) are transferred to the computer (a) for storage. Signals are recorded for a finite length of time, depending on the decay rate for the NMR signal and operational objectives.

The multicoil NMR data acquisition experiment is repeated using a sufficient number of different transmit array combinations and transmitted energy levels to achieve the desired spatial resolution.

Embodiments and variations of the multicoil NMR data acquisition method:

A first embodiment of the multicoil data acquisition method is to transmit on only one transmit coil for each single NMR measurement. A series of such measurements are acquired using different transmit coils, and using at least two different transmit energy levels for each selected transmit coil.

A second embodiment of the multicoil NMR data acquisition method is to transmit simultaneously on all of the transmit coils, but to use at least two linearly independent transmit array combinations, and at least two different total transmitted energy levels for each transmit array combination.

A preferred embodiment of the multicoil NMR data acquisition method uses the same array of coils for both the transmit function and the receive function. Turning then to FIG. 2, a switching circuit ($d_1 - d_N$) is located at or near the drive point of each coil. In this embodiment, the switching circuits ($d_1 - d_N$) isolate the sensitive receive electronics during the application of the high-energy transmit pulse(s). The tuning circuits ($e_1 - e_N$) may be switched to a low-Q state during the short period between the end of the transmit pulse and the onset of data recording, to allow transient coil currents to dissipate.

Another embodiment of the multicoil NMR data acquisition method utilizes a reduced number of transmit and/or receive coils, and utilizes repeated measurements physically displacing the coils between measurements, in order to synthesize a larger transmit and/or receive array. This embodiment might be preferred in applications where the savings in cost

and complexity for the acquisition hardware outweighs the additional time that it might take to collect the required measurements in synthetic aperture mode. Another potential benefit of synthetic aperture processing is reduction or elimination of mutual coupling between the receive coils, especially if the embodiment uses a single receive coil.

5 A preferred embodiment of the multicoil NMR data acquisition method is to utilize single or multiple-turn wire loops as the transmit coils and/or receive coils. However, those persons skilled in the art will appreciate that any transmit device capable of generating an alternating magnetic field, and any receive device capable of measuring an alternating magnetic field can be employed. Thus, alternative transmit devices include any viable means for creating
10 a magnetic field, such as current carrying loops, coils (whether open core or filled core, e.g., iron), long lines, etc. Alternative receive devices include loops, coils or other similar apparatus capable of transmitting induced electrical currents, magnetometers, e.g., flux gate, magneto-resistive, etc., interference devices such as superconducting quantum interference apparatus.

A preferred embodiment of the multicoil NMR data acquisition method is to transmit a
15 single continuous pulse, and then record the resulting free induction decay (FID) signals on the receive coils. The multicoil NMR data acquisition method may also be embodied by transmitting a series of plural pulses to produce spin-echo signals on the receive coils. Those persons skilled in the art will appreciate that embodiments of the invention are not limited to any particular transmitted waveform, or to any particular series of transmitted waveforms;
20 multicoil NMR data acquisition methods according to the invention may use any combination of transmitted waveforms that will produce a useable NMR signal on the receive coil(s).

Data Processing Method:

The present invention specifies three different methods for mathematically processing
25 the multicoil NMR data, acquired according to the multicoil NMR data acquisition method, to isolate the NMR signals arising from different regions of the three-dimensional volume of investigation. The first method is an application of the principle of matched filtering (correlation) for multicoil NMR imaging. The second method is an application of adaptive filtering for multicoil NMR imaging. The third method is the application of linear inverse/least
30 squares solution techniques for multicoil NMR imaging.

In all three data processing methods, the data consists of a set of $L \times M \times P$ sampled NMR signals, where L is the number of different transmit array combinations, M is the number

of receive coils, and P is the number of different total energy levels transmitted for each transmit array combination. If each NMR signal consists of K time-domain data samples, then the entire data set consists of $K \times L \times M \times P$ data samples.

5 *Detailed description of the matched filtering data processing method:*

The generic method of mathematical correlation is familiar to those skilled in the arts of math and science. The embodiment described in the following paragraphs includes a specific formulation of the correlation method for estimating the three-dimensional NMR spin density distribution, given a set of NMR data acquired using the multicoil NMR data acquisition method.

10 The relative NMR spin density is estimated on a point-by-point basis, throughout the three-dimensional volume of interest. The volume may be sampled uniformly or non-uniformly, depending on the requirements of the application. For each hypothetical sample location (a location in the volume of interest), the relative NMR spin density is estimated as follows:

1. Compute the hypothetical initial amplitudes and phases, for the entire set of $L \times M \times P$ sampled NMR signals, that would occur if a standardized unit volume of NMR spin density centered at the hypothetical sample location was subjected to the same multicoil NMR data acquisition procedure that is used to generate the data. For a single sampled NMR signal, this is accomplished by the following procedure, which will be understood by those who are skilled in the art of NMR processes and antenna field theory:
 - 20 i) Compute the phase of the precessing magnetic moment at the hypothetical sample location, relative to a fixed reference phase. The phase of the precessing magnetic moment is determined by the orientation of the transverse component of the transmitted B1 field at the hypothetical sample location. (In this discussion, the transverse component of any field is the component of the field that is perpendicular to the static field B0.)
 - 25 ii) Compute the phase of the received NMR signal due to the assumed precessing magnetic moment at the hypothetical sample location. The phase of the received NMR signal is determined by the orientation of the transverse component of the

receive coil at the hypothetical sample location, the phase of the precessing magnetic moment, and the fixed phase reference.

- 5 iii) Compute the tip angle of the precessing magnetic moment at the hypothetical sample location. The tip angle is determined by the total energy contained in the transverse field component of the transmitted pulse, at the hypothetical sample location. For a single transmit pulse, the tip angle is generally a linear function of the energy contained in the transverse component of the field at the sample location. If multiple transmit pulses are used, the tip angle depends on the entire pulse train.
- 10 iv) Compute the initial amplitude of the received NMR signal. The initial amplitude of the received NMR signal depends on the magnitude of the transverse component of the receive coil field at the hypothetical sample location, as well as the tip angle of the precessing magnetic moment. The initial amplitude of the received NMR signal is a sinusoidal function of the tip angle, with maxima at +90 degrees and -90 degrees, and minima at 0 degrees and +180 degrees.
- 15 v) The entire set of $L \times M \times P$ initial received amplitude and phase values may be arranged as a $L \times M \times P$ vector of complex numbers, where each complex number represents the hypothetical initial amplitude and phase of one of the NMR signals for the hypothetical sample location. This vector represents a filter vector that is matched to the expected set of initial amplitudes and phases for a unit volume of
- 20 NMR spin density at the hypothetical sample location. This matched filter vector is referred to as $h_{(x,y,z)}$, where the subscript (x,y,z) denotes the hypothetical sample location in Cartesian coordinate space.
2. Compute the 2-norm $\| h_{(x,y,z)} \|$ of the matched filter vector $h_{(x,y,z)}$.
 3. Normalize the matched filter vector $h_{(x,y,z)}$ to unit energy by dividing it, sample-by-sample, by its 2-norm:
- 25

$$h_{n(x,y,z)} = h_{(x,y,z)} / \| h_{(x,y,z)} \|.$$

- 30 4. Multiply each of the measured NMR signals by the associated initial amplitude sample from the normalized matched filter vector $h_{n(x,y,z)}$.
5. Apply a constant phase shift to each of the measured NMR signals equal to the negative of the associated phase sample from the normalized matched filter vector $h_{n(x,y,z)}$.

6. Coherently sum, on a time sample-by-sample basis, all of the amplitude-adjusted phase-shifted versions of the measured NMR signals. The resulting composite sampled NMR signal $s_{(x,y,z)}$ is the estimated NMR signal for the hypothetical sample location (x,y,z) .
7. The relative NMR spin density at the location (x,y,z) is estimated as the initial value of $s_{(x,y,z)}$ divided by $\|h_{(x,y,z)}\|$.

Features of this technique are the construction of the matched filter $h_{(x,y,z)}$, and its application to isolate the NMR signal $s_{(x,y,z)}$ arising from a given location (x,y,z) within the volume. Other relevant sample properties, such as the decay constant at location (x,y,z) , can be estimated from the composite NMR signal $s_{(x,y,z)}$ using existing signal processing methods, which are familiar to those skilled in the art of NMR.

Embodiments using the matched filtering data processing method:

In a preferred embodiment using the matched filtering data processing method, the phase shift is implemented by applying a time shift to each measured NMR signal such that the signal phase at the Larmor frequency is shifted by the specified amount. In another variation, the time shift is accomplished in the Fourier domain by computing the discrete Fourier transform of the measured NMR signal, then applying a linear phase shift in the Fourier domain, and then computing the inverse Fourier transform to produce the time-shifted version of the measured NMR signal.

In another preferred embodiment using the matched filtering data processing method, the measured NMR signals are de-modulated by multiplication with the sampled exponential function $e^{(-j2\pi f t T)}$, where f is the Larmor frequency. In this embodiment, the measured NMR signals are transformed to complex valued sequences centered approximately at DC. In this variation, the phase shift of the matched filter is applied directly to each complex NMR signal by multiplying each time-domain sample by $e^{(j\phi)}$ or $e^{(-j\phi)}$, where ϕ is phase of a matched filter for that particular NMR signal.

In yet another embodiment using the matched filtering data processing method, each measured NMR signal is initially reduced to a single complex number by multiplying it by the sampled exponential function $e^{(-j2\pi f t T)}$ and coherently summing the series of samples (or equivalently, computing the discrete Fourier transform of the series and selecting the DFT

sample at the Larmor frequency). This complex number is an estimate of the amplitude and phase of the NMR signal content at the Larmor frequency. In this embodiment, the matched filter phase shift is applied by multiplying the single complex number representing each measured NMR signal by $e^{j\phi}$ or $e^{-j\phi}$, where ϕ is phase of a matched filter for that particular
 5 NMR signal.

In still another embodiment using the matched filtering data processing method, the discrete sine transform is used to execute the portion of the matched filtering relating to the sinusoidally-dependent NMR tip angle response.

10 *Detailed description of the adaptive filtering data processing method:*

The generic method of adaptive filtering is familiar to those persons skilled in the art of math and signal processing. Embodiments of the invention use a specific formulation of the adaptive filtering method for estimating the three-dimensional NMR spin density distribution,
 15 given a set of NMR data acquired using the multicoil NMR data acquisition method.

The relative NMR spin density is estimated on a point-by-point basis, throughout the three-dimensional volume of interest. The volume may be sampled uniformly or non-uniformly, depending on the requirements of the application. For each hypothetical sample location (a location in the volume of interest), the relative NMR spin density is estimated as
 20 follows:

1. Arrange the entire set of measured NMR data as a matrix \mathbf{B} with K columns and $L \times M \times P$ rows. Each row is one measured, sampled NMR signal, corresponding to one particular combination of transmit array combination, receive coil(s) and transmit
 25 energy. The column indices correspond to time samples.
2. Compute the data correlation matrix for the measured data matrix:

$$\mathbf{R}_{\mathbf{B}\mathbf{B}} = \mathbf{B}\mathbf{B}^{\mathbf{H}}$$

30 where the superscript \mathbf{H} denotes conjugate transpose.

3. If the correlation matrix \mathbf{R}_{BB} is less than full rank, pre-process \mathbf{R}_{BB} so that it becomes invertible (full rank). One method for making \mathbf{R}_{BB} invertible is to average the all the matrix elements along each diagonal.
4. Compute the inverse $\mathbf{R}_{\text{BB}}^{-1}$ of the full-rank data correlation matrix \mathbf{R}_{BB} .
5. For each hypothetical sample location (x,y,z) , compute the normalized matched filter vector $h_{n(x,y,z)}$ as previously described in the detailed description for the matched filtering method (1. i – v).
6. Compute the adaptive filter $m_{(x,y,z)}$ as

$$m_{(x,y,z)} = h_{n(x,y,z)} \mathbf{R}_{\text{BB}}^{-1} / (h_{n(x,y,z)} \mathbf{R}_{\text{BB}}^{-1} h_{n(x,y,z)}^H)^{1/2}.$$

7. Multiply each of the measured NMR signals by the associated initial amplitude sample from the adaptive filter vector $m_{(x,y,z)}$.
8. Apply a constant phase shift to each of the measured NMR signals equal to the negative of the associated phase sample from the adaptive filter vector $m_{(x,y,z)}$.
9. Coherently sum, on a time sample-by-sample basis, all of the amplitude-adjusted phase-shifted versions of the measured NMR signals. The resulting composite sampled NMR signal $s_{(x,y,z)}$ is the estimated NMR signal for the hypothetical sample location (x,y,z) .

Features of this technique are the construction of the adaptive filter $m_{(x,y,z)}$, and its application to isolate the NMR signal $s_{(x,y,z)}$ arising from a given location (x,y,z) within the volume. Other relevant sample properties, such as the decay constant at location (x,y,z) , can be estimated from the composite NMR signal $s_{(x,y,z)}$ using existing signal processing methods, which are familiar to those skilled in the art of NMR.

The difference between the normalized matched filter $h_{n(x,y,z)}$ and the adaptive filter $m_{(x,y,z)}$ is that the matched filter is optimized for detecting the NMR signal emanating from location (x,y,z) in a background of random white noise, while the adaptive filter is optimized for isolating the NMR signal emanating from location (x,y,z) when the interference signal exhibits a correlated structure in the measured data.

Embodiments using the adaptive filtering data processing method:

In a preferred embodiment using the adaptive filtering data processing method, the phase shift is implemented by applying a time shift to each measured NMR signal such that the signal phase at the Larmor frequency is shifted by the specified amount. In another variation, the time shift is accomplished in the Fourier domain by computing the discrete Fourier
5 transform of the measured NMR signal, then applying a linear phase shift in the Fourier domain, and then computing the inverse Fourier transform to produce the time-shifted version of the measured NMR signal.

In another preferred embodiment using the adaptive filtering data processing method, the measured NMR signals are de-modulated by multiplication with the sampled exponential
10 function $e^{(j2\pi fnT)}$, where f is the Larmor frequency. In this embodiment, the measured NMR signals are transformed to complex valued sequences centered approximately at DC. In this variation, the phase shift of the adaptive filter is applied directly to each complex NMR signal by multiplying each time-domain sample by $e^{(j\phi)}$ or $e^{(-j\phi)}$, where ϕ is phase of adaptive filter for that particular NMR signal.

In yet another embodiment using the adaptive filtering data processing method, each
15 measured NMR signal is initially reduced to a single complex number by multiplying it by the sampled exponential function $e^{(-j2\pi fnT)}$ and coherently summing the series of samples (or equivalently, computing the discrete Fourier transform of the series and selecting the DFT sample at the Larmor frequency). This complex number is an estimate of amplitude and phase
20 of the NMR signal content at the Larmor frequency. In this embodiment, any time-domain envelope information, such as the exponential decay rate, is lost. In this embodiment, the adaptive filter phase shift is applied by multiplying the single complex number representing each measured NMR signal by $e^{(j\phi)}$ or $e^{(-j\phi)}$, where ϕ is phase of adaptive filter for that particular NMR signal.

25

Detailed description of the linear inverse/least-squares data processing method:

The generic method of computing a solution to a set of linear equations is familiar to those persons skilled in the art of math and science. Embodiments of the invention employ a
30 specific formulation of the linear inverse/least squares solution technique for estimating the three-dimensional NMR spin density distribution, given a set of NMR data acquired using the multi-channel data acquisition method.

The linear inverse/least-squares data processing method for estimating the 3-D NMR spin density from a set of multi-channel NMR data is implemented as follows:

- 5 1. Select a set discrete volume elements (voxels) that encompass the 3-D volume or object of interest. The voxel sizes and shapes may be uniform (i.e. cubes of fixed dimension), variable, or arbitrary.
2. Develop a set of linear equations $Ax = b$ relating the unknown sampled NMR signal arising from the spin density within each voxel, to each sample in the measured data set. This may be accomplished as follows:
 - 10 a. Model the sampled NMR signal source in each voxel as a set of time-domain samples. The NMR signal source in each voxel has an unknown initial amplitude that is dependent on the volume contained by the voxel and the NMR spin density within the voxel. The NMR signal source also has an unknown initial phase and unknown time-domain modulation. The phase and time
15 domain modulation (including decay rates) are characteristic properties the material within each voxel.
 - b. Compute the coefficients for the set of linear equations relating the unknown NMR signal source samples for each voxel to the measured data samples. These coefficients depend on the amplitudes and phases of the transverse magnetic
20 fields of the receive coils at each voxel, and the sequence of applied transverse B1 pulse energies at each voxel. The linear transform coefficients can be calculated using the description for the matched filtering method (1. i – v), along with a model for the absolute initial amplitude of the received signal based on the dimension of each voxel.
 - 25 c. Organize the system of linear equations as a matrix equation:

$$Ax = b$$

30 where x is the vector of unknown NMR signal source samples (N time-domain samples for each voxel), b is the vector of measured NMR data samples, and A is the matrix of coefficients relating the unknown voxel-specific time-domain samples x to the measured NMR data samples b .

3. Compute the least squares solution to $Ax = b$, or a regularized version of the least squares solution to $Ax = b$. There are many possible methods for computing the least squares solution or a regularized least squares solution to a set of linear equations. Thus, any mathematical algorithm that computes an estimate of the least squares solution or regularized least squares solution to the set of linear equations $Ax = b$ is considered an appropriate means for solving the equation. Specific embodiments are described hereinafter.

Embodiments using the linear inverse/least-squares data processing method:

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In a preferred embodiment using the linear inverse/least-squares data processing method, the least squares solution x is computed directly using via the least squares pseudo-inverse:

$$15 \quad x = (A^H A)^{-1} A^H b$$

where the superscript H indicates conjugate transpose. In a preferred variation of this embodiment, the least squares solution is regularized by adding a constant scalar value to the diagonal elements of A or $A^H A$, prior to computing the inverse of $(A^H A)$.

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In another preferred embodiment using the linear inverse/least-squares data processing method, the least squares solution is computed by first computing the singular value decomposition of A as

$$25 \quad A = USV^H,$$

where the columns of V are an orthonormal set of basis vectors for $A^H A$ and the elements w_j of the diagonal matrix S contains the positive square roots of the eigenvalues of $A^H A$, and then computing the least squares solution as:

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$$x = V[\text{diag}(1/w_j)]U^H b .$$

In a preferred variation of this embodiment, the least squares solution is regularized by weighting the orthogonal solution components such that the solution components generated from columns V with large associated singular values (w_j) are emphasized more than the solution components generated from columns of V with small associated singular values.

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In yet another preferred embodiment using the linear inverse/least-squares data processing method, the least squares solution is computed using a linear iterative algorithm. Such linear iterative solution techniques include, but are not limited to: the Gradient Descent algorithm, the Steepest Descent algorithm, and the Conjugate Gradient algorithm. In a preferred variation of this embodiment, the least squares solution is regularized by terminating the iteration prior to its final convergence to the least squares solution.

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In still another embodiment using the linear inverse/least-squares data processing method, each measured NMR signal is initially reduced to a single complex number by multiplying it by the sampled exponential function $e^{-j2\pi f_n T}$ and coherently summing the series of samples (or equivalently, computing the discrete Fourier transform of the series and selecting the DFT sample at the Larmor frequency). This complex number is an estimate of the amplitude and phase of the NMR signal content at the Larmor frequency. In this embodiment, any time-domain envelope information, such as the exponential decay rate, is lost. In this embodiment, the solution x consists of complex samples, where each sample represents the amplitude and phase of the NMR signal source for a given voxel.

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OPERATION OF A ROBUST EMBODIMENT

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While the invention comprises at least some of the previously described features in various combinations, a better understanding of the invention can be ascertained by reviewing the field implementation of many of these features. Thus, the general procedure for acquiring and processing NMR data using this invention consists of: (1) hardware set-up, (2) data acquisition, (3) data processing.

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- 1) Hardware set-up preferably comprises arranging the transmit coils and receive coils in a pattern near or around the object or volume of interest, and arranging the other

acquisition hardware so as not to interfere with the data collection procedure. The coils may be arranged to maximize coverage of the object or volume of interest, and/or to maximize the diversity of coil field patterns incident across the object or volume of interest. Furthermore, the coil arrays may be arranged to minimize mutual coupling between coils. In addition, the layout of the coil arrays may be accomplished with the aid of numerical modeling software to optimize the resulting image quality for each application. Other acquisition devices should be arranged so as not to produce undue electrical or magnetic interference that would degrade the quality of the recorded NMR data.

- 2) Data acquisition preferably comprises transmitting specified magnetic pulse trains at the Larmor frequency, using at least two transmit coils, and recording the subsequent NMR signals from at least two receive coils. Data are recorded, digitized and stored on appropriate media as the data acquisition progresses.
- 3) Data processing preferably comprises executing computer software that retrieves the stored NMR data and processes it using one of the three data processing methods described herein so as to estimate the NMR spin density distribution and other material properties within the three-dimensional volume. Data processing may be performed entirely after all the NMR data for a given investigation have been acquired and stored. Alternately, data processing may be performed intermittently, in parallel with the data acquisition procedure, as partial NMR data becomes available.

With respect to the above description then, it is to be realized that the optimum dimensional relationships for the parts of the invention, to include variations in size, materials, shape, form, function and manner of operation, assembly and use, are deemed design and optimization considerations readily apparent and obvious to a person skilled in the art, and all equivalent relationships to those illustrated in the drawings and described in the specification are intended to be encompassed by the present invention.

Therefore, the foregoing is considered as illustrative only of the principles of the invention. Further, since numerous modifications and changes will readily occur to those skilled in the art, it is not desired to limit the invention to the exact construction and operation shown and described, and accordingly, all suitable modifications and equivalents may be resorted to, falling within the scope of the invention.

What is claimed:

1. A method of constructing a 3-dimensional nuclear magnetic resonance image of at least a portion of a target without generating gradients in a static magnetic field, comprising:
 - 5 a) relying upon environmentally innate static magnetic field gradients and using a plurality of magnetic field generating coils with spatially distinct magnetic field patterns, transmitting alternating magnetic field pulses at the Larmor frequency of the target using a plurality of linearly independent combinations of relative current amplitudes and/or phases among the transmitting coils, and using P different values
10 of total transmitted energy for each combination of transmit coils used, where $P > 1$;
 - b) using a plurality of magnetic field receiving coils with spatially distinct magnetic field patterns, detecting and recording a set of nuclear magnetic resonance signals arising from each transmit pulse, each of the set of nuclear magnetic resonance signals comprising a plurality of samples;
 - 15 c) arranging the set of recorded nuclear magnetic resonance data samples as a vector b ; and
 - d) reconstructing a 3-dimensional nuclear magnetic resonance image wherein each sampled location in the 3-dimensional image space is assigned a scalar value s , wherein the scalar value s is computed as a weighted linear combination of the
20 recorded data samples b : $s = \sum_j w_j b_j$
2. The method according to claim 1, wherein the scalar value for a sampled location in the 3-dimensional image is computed using a matched filtering data processing method comprising:
 - 25 a) arranging the set of recorded nuclear magnetic resonance data samples as a vector b ;
 - b) computing the expected tip angle and phase of a precessing unit-valued magnetic moment at the hypothetical sample location, for each applied combination of magnetic field transmitting coils and pulse energies;
 - c) computing the expected amplitude and phase of each nuclear magnetic resonance
30 data sample, each data sample resulting from the detection of the precessing unit-valued magnetic moment at the hypothetical sample location by each of magnetic field receiving coils;

- d) arranging the set of the computed data samples as a vector matched filter vector h ;
- e) computing a conjugate matched filter vector h^* formed as a complex conjugate value of h ; and
- f) computing the scalar value s for the sample location as the cross-correlation between the conjugate matched filter vector h^* and the experimentally recorded nuclear magnetic resonance data samples b : $s = \sum_j h_j^* b_j$
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3. The method according to claim 1, wherein the scalar value for a sampled location in the 3-dimensional image is computed using an adaptive filtering data processing method comprising:
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- a) computing a matched filter vector h according to claim 2;
- b) arranging the set of recorded nuclear magnetic resonance data as a matrix \mathbf{B} with $M \times L \times P$ rows, wherein each row is one sampled nuclear magnetic resonance signal recorded at one magnetic field receiving coil for one combination of transmitting coils and transmitted pulse energies;
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- c) computing a data correlation matrix $\mathbf{R}_{\mathbf{B}\mathbf{B}} = \mathbf{B}\mathbf{B}^{\mathbf{H}}$ where the superscript \mathbf{H} denotes conjugate transpose;
- d) computing the inverse $\mathbf{R}_{\mathbf{B}\mathbf{B}}^{-1}$ of the full-rank data correlation matrix $\mathbf{R}_{\mathbf{B}\mathbf{B}}$;
- 20
- e) computing the adaptive filter vector $m = h \mathbf{R}_{\mathbf{B}\mathbf{B}}^{-1} / (h \mathbf{R}_{\mathbf{B}\mathbf{B}}^{-1} h^{\mathbf{H}})^{1/2}$;
- f) computing a conjugate adaptive filter vector m^* formed as a complex conjugate value of m ; and
- g) computing the scalar value s for the sample location as the cross-correlation between the conjugate adaptive filter vector m^* and the experimentally recorded nuclear magnetic resonance data samples b :
- 25

$$s = \sum_j m_j^* b_j$$

4. The method according to claim 1, wherein the scalar value for a sampled location in the 3-dimensional image is computed using a linear inverse/least-squares data processing method comprising:
- 30

- a) selecting a set of discrete volume elements (voxels) that encompass the 3-D volume or object of interest; and
- b) developing a set of linear equations $Ax = b$ relating the sampled signal arising from the unknown spin density within each individual voxel to each sample in the experimentally recorded data set comprising:
- 1) arranging the entire set of recorded nuclear magnetic resonance data samples as a vector b ;
 - 2) arranging the set of unknown voxel spin density values as a vector x ;
 - 3) computing each coefficient of the matrix A as a complex value describing the amplitude and phase of the recorded sample of b that would result from the detection of a collection of precessing nuclear magnetic resonance spins, of unit spin density, contained within the hypothetical voxel corresponding to an unknown sample of x ;
 - 4) calculating the least squares solution to the system of linear equations $Ax = b$, or calculating a regularized least squares solution to $Ax = b$, using any mathematical algorithm that computes an estimate of the least squares solution or regularized least squares solution to the set of linear equations $Ax = b$.
5. The method according to claim 2, wherein the matched filter vector h is normalized to unit energy.
6. The method according to claim 3, wherein the adaptive filter vector m is normalized to unit energy.
7. The method according to claim 4, wherein the least squares solution is calculated by one of the direct pseudo-inverse $x = (A^H A)^{-1} A^H b$, or by the regularized direct pseudo-inverse, where small scalar values are added to the diagonal elements of A or $A^H A$, prior to computing the inverse of $(A^H A)$.
8. The method according to claim 4, wherein the least squares solution or regularized least squares solution is calculated by a singular value decomposition method comprising:

- a) calculating the singular value decomposition of the matrix $\mathbf{A} = \mathbf{U}\mathbf{S}\mathbf{V}^{\mathbf{H}}$; and
- b) one of calculating the least squares solution as $x = \mathbf{V}[\mathit{diag}(1/\sigma_j)]\mathbf{U}^{\mathbf{H}}b$, or calculating a weighted least squares solution, where the diagonal terms $\mathit{diag}(1/\sigma_j)$ are each multiplied by a weighting factor prior to performing the matrix multiplication.

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9. The method according to claim 4, wherein the least squares solution or regularized least squares solution is calculated using a linear iterative least squares solution algorithm comprising:
 - a) the gradient descent algorithm;
 - 10 b) the steepest descent algorithm; or
 - c) the conjugate-gradient algorithm.
10. The method according to any of claims 1 – 4 wherein at least some the nuclear magnetic resonance signals result from the presence of groundwater.
- 15 11. The method according to any of claims 1 – 4 wherein the static magnetic field gradient is the Earth's magnetic field.
12. The method according to any of claims 1 – 4 wherein the transmitting magnetic field coils and receiving magnetic field coils are conducting loops of one or more turns.
- 20 13. The embodiment of claims 1 – 4 wherein at least one of the transmitting magnetic field coils and receiving magnetic field coils is the same.
- 25 14. The method according to any of claims 1 – 4 wherein a reduced number of transmitting magnetic field coils and/or receiving magnetic field coils are physically displaced and additional nuclear magnetic resonance signals are recorded via the displaced coils, so as to generate a set of data equivalent to that obtained using a full set of transmitting and receiving magnetic field coils.

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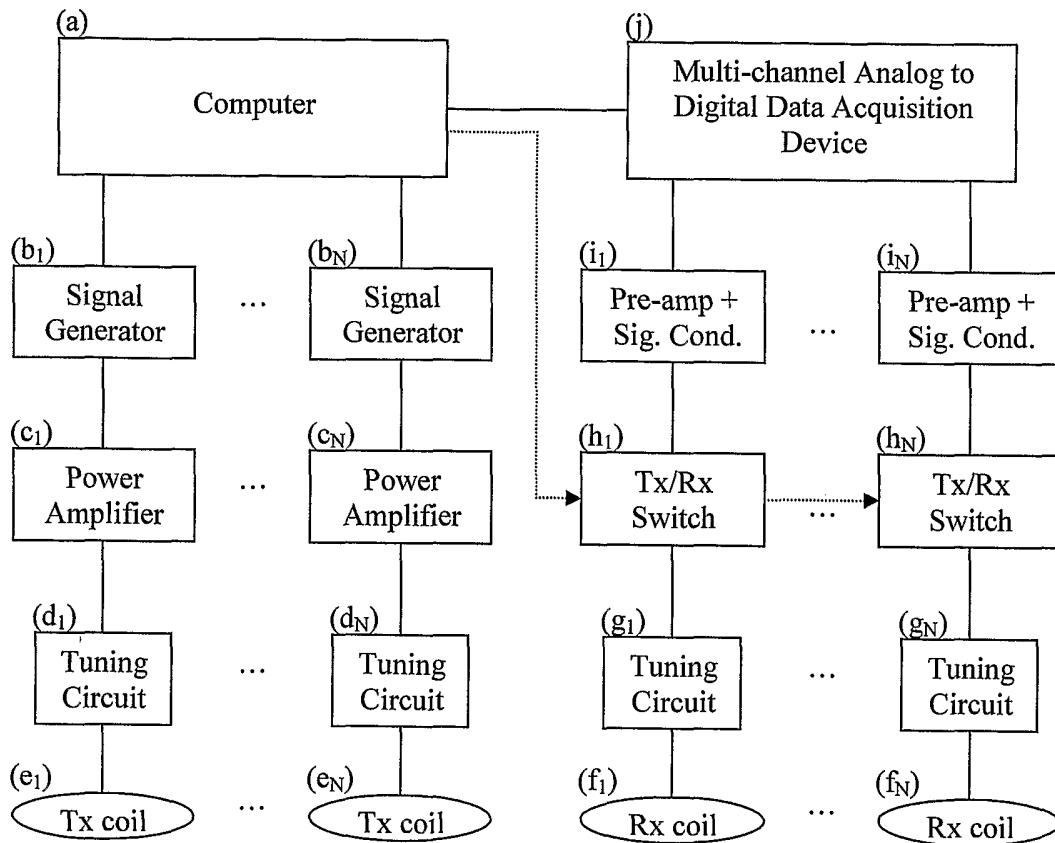


FIG. 1

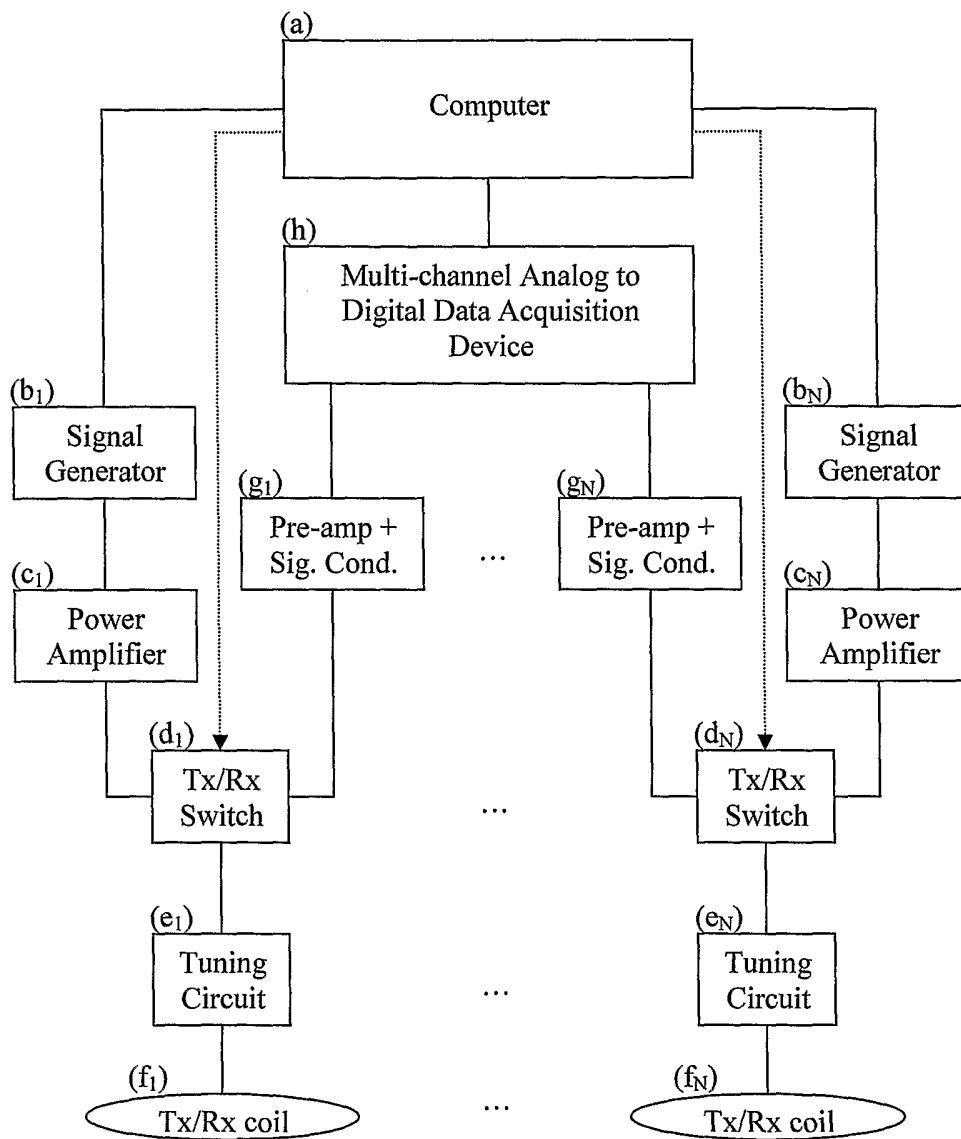


FIG. 2

INTERNATIONAL SEARCH REPORT

International Application No

PCT/US2004/021911

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No
A	C.E. HAYES ET AL.: "VOLUME IMAGING WITH MR PHASED ARRAYS" MAGNETIC RESONANCE IN MEDICINE, vol. 18, 1 April 1991 (1991-04-01), pages 309-319, XP000209845 ISSN: 0740-3194 pages 309 - 316: "Introduction" and "Methods" -----	1-4, 12-14
A	US 5 759 152 A (J. FELMLEE, J.P. DEBBINS) 2 June 1998 (1998-06-02) column 2, line 48 - column 3, line 44 column 4, line 23 - line 46 column 5, line 8 - line 60 -----	1

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No PCT/US2004/021911

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
EP 0170508	A	05-02-1986	DE 3579771 D1 25-10-1990
			EP 0170508 A2 05-02-1986
			US 4727324 A 23-02-1988
US 6160398	A	12-12-2000	NONE
US 5759152	A	02-06-1998	NONE