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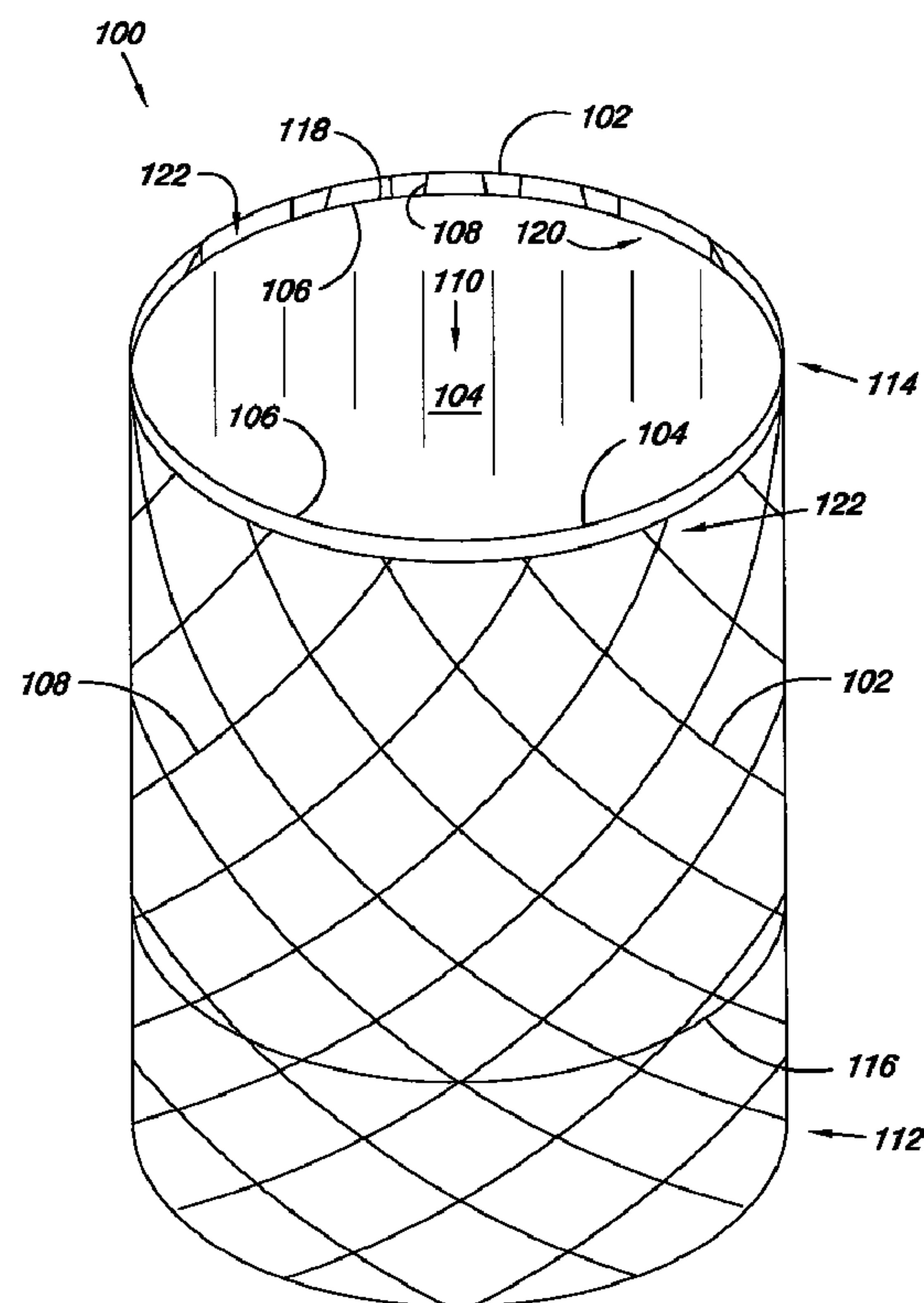


Fig. 1

(57) **Abrégé/Abstract:**

A valve (100) for use in a body lumen, where the valve includes a valve leaflet (104) with delayed leaflet deployment relative an in vivo implant time. The valves includes a valve frame (102), a valve leaflet (104) coupled to the valve frame. The valve leaflet includes



(57) **Abrégé(suite)/Abstract(continued):**

a commissure (106) that can reversibly seal for unidirectional flow of a liquid through the valve, and a biodegradable adhesive (122) between the valve leaflet and the valve frame to hold at least the commissure of the valve leaflet in a static relationship relative the valve frame for a predetermined time once implanted in vivo.

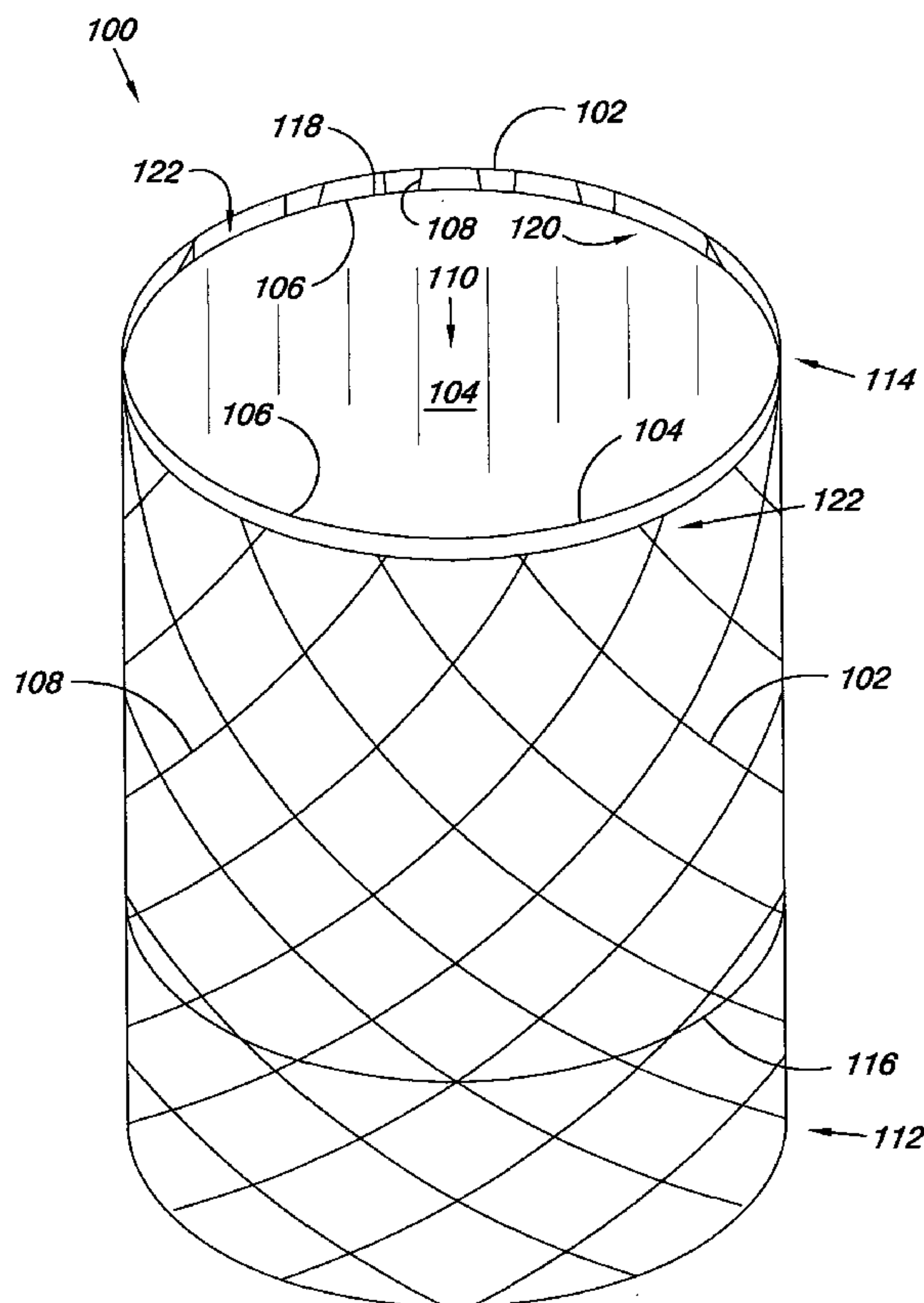


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Fig. 1



(57) Abstract: A valve (100) for use in a body lumen, where the valve includes a valve leaflet (104) with delayed leaflet deployment relative an in vivo implant time. The valves includes a valve frame (102), a valve leaflet (104) coupled to the valve frame. The valve leaflet includes a commissure (106) that can reversibly seal for unidirectional flow of a liquid through the valve, and a biodegradable adhesive (122) between the valve leaflet and the valve frame to hold at least the commissure of the valve leaflet in a static relationship relative the valve frame for a predetermined time once implanted in vivo.

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VALVE WITH DELAYED LEAFLET DEPLOYMENT

Technical Field

The present disclosure relates generally to a valve for use in a body lumen,
5 and more particularly to a valve having a valve leaflet with delayed leaflet
deployment relative an in vivo implant time.

Background

Heart failure is rapidly becoming one of the most common cardiovascular
10 disorders. Unfortunately, an optimal treatment for heart failure has not yet been
determined.

Generally, heart failure is classified as a syndrome which develops as a
consequence of cardiac disease, and is recognized clinically by different signs and
symptoms that are produced by complex circulatory and neuro-hormonal responses to
15 cardiac dysfunction.

Dysfunction in one or both of the systolic function and/or the diastolic
function of the heart can lead to heart failure. For example, left ventricular diastolic
dysfunction is recognized as a condition leading to morbidity, hospitalizations and
death. Left ventricular diastolic dysfunction is a condition in which the left ventricle
20 of the heart exhibits a decreased functionality. This decreased function could lead to
congestive heart failure or myocardial infarction, among other cardiovascular
diseases.

Treatment of left ventricular diastolic dysfunction can include the use of
pharmaceuticals. Despite these treatments, improving the approach to treating
25 diastolic dysfunction continues to be a goal of the medical community.

Brief Description of the Drawings

Figure 1 illustrates an embodiment of a valve of the present disclosure.

Figure 2A illustrates an embodiment of a system having a valve of the present
30 disclosure.

Figure 2B illustrates an embodiment of a system having a valve of the present
disclosure.

Detailed Description

Embodiments of the present disclosure are directed to a valve having a valve leaflet, a system that includes the valve, and a method of making and/or using the valve. For the embodiments, the valve leaflet has a delayed deployment relative an in vivo implant time of the valve. For the embodiments, the delayed deployment can be accomplished through the use of a biodegradable adhesive (e.g., a biodegradable material) that holds the valve leaflet in a static relationship relative the valve frame for a predetermined time. Once implanted in vivo, the biodegradable adhesive degrades and/or erodes over the predetermined time to at least the point where the valve leaflet is released from its static relationship relative the valve frame. Once released, the valve leaflet can then operate to control the flow of a fluid through the valve in an essentially unidirectional manner.

As used herein, the terms "a," "an," "the," "one or more," and "at least one" are used interchangeably and include plural referents unless the context clearly dictates otherwise. Unless defined otherwise, all scientific and technical terms are understood to have the same meaning as commonly used in the art to which they pertain. For the purpose of the present disclosure, additional specific terms are defined throughout.

As used herein, the "valve" can be formed from a number of metals, metal alloys, biological materials and/or synthetic materials. For example, the valve leaflet can be formed from one or more of a biological material (e.g., a non-autologous material) and/or a synthetic material (e.g., a synthetic polymer) having suitable mechanical and material properties. In addition, the valve frame can be formed from a synthetic material, a metal and/or a metal alloy having suitable mechanical and material properties. Other materials are also possible. The materials used in forming the valve will be discussed more fully herein.

The valve of the present disclosure can be implanted in one or more vessels of a mammal (e.g., a human) body where it would be desirable to allow the valve frame to first seat (e.g., anchor) and be at least be partially in-grown at the implant site before exposing the valve to forces imparted through the opening and closing of the valve leaflet. For the various embodiments, the valve leaflets maintain their "open" configuration (i.e., their static relationship relative the valve frame) through the use of the biodegradable adhesive, as discussed herein. In this "open" configuration

longitudinal shear stresses through the valve can be minimized, allowing the valve frame to seat and be in-grown at the implant site over the predetermined time.

As used herein, the one or more "vessels" can include vessels of the cardiovascular system (e.g., arteries and veins), which can include both the coronary and/or the peripheral vasculature, vessels of the lymphatic system, vessels and/or ducts of the urinary system, and/or vessels and/or ducts of the kidney system. Other vessel locations within the mammal body for implanting the valve of the present disclosure are also possible.

The figures herein follow a numbering convention in which the first digit or digits correspond to the drawing figure number and the remaining digits identify an element or component in the drawing. Similar elements or components between different figures may be identified by the use of similar digits. For example, 110 may reference element "10" in Fig. 1, and a similar element may be referenced as 210 in Fig. 2. As will be appreciated, elements shown in the various embodiments herein can be added, exchanged, and/or eliminated so as to provide any number of additional embodiments of valve and/or system. In addition, as will be appreciated the proportion and the relative scale of the elements provided in the figures are intended to illustrate the embodiments of the present disclosure, and should not be taken in a limiting sense.

Various non-limiting embodiments of the present disclosure are illustrated in the figures. Generally, the valve can be implanted within a vessel to regulate the flow of a bodily fluid through the body lumen in a single direction.

Figure 1 provides an embodiment of a valve 100 that includes a valve frame 102 and a valve leaflet 104 coupled to the valve frame 102. As illustrated, the valve 100 can be formed with a valve leaflet 104 having a commissure 106 that can reversibly seal for unidirectional flow of a liquid through the valve 100. As discussed herein, embodiments of the valve 100 having one leaflet 104 or more than two leaflets 104 are possible.

The valve frame 102 also includes frame members 108 that help to define a lumen 110. For the various embodiments, the valve frame 102 can have an elongate tubular structure with a proximal end 112 and a distal end 114. For the various embodiments, portions of the frame members 108 define the proximal and distal ends 112, 114 of the valve frame 102.

The valve leaflet 104 also has a proximal end 116 and a distal end 118. As illustrated, the proximal end 116 of the leaflet 104 can be coupled to the valve frame 102 through a number of different techniques. For example, the material 120 forming the leaflet 104 can be stitched, bonded, glued or otherwise secured to the valve frame 102 so as to form the proximal end 116 of the valve leaflet 104. In one embodiment, the material 120 can be secured to the valve frame 102 at a position that is at or adjacent the proximal end 112. Alternatively, the material 120 can be secured to the valve frame 102 at a position that is between the proximal and distal ends 112, 114 of the valve frame 102. For the various embodiments, the material 120 forming the valve leaflet 104 can define at least a part of the lumen 110 of the valve 100.

As illustrated, the distal end 118 of the valve leaflet 104 includes the commissure 106 that can reversibly form to control fluid flow through the valve 100. As used herein, the commissure 106 is the location of the valve leaflet 104 that releasably join and seal to allow for unidirectional flow through the valve 100. As illustrated, the commissure 106 is approximately adjacent the distal end 118 of the valve leaflet 104.

As illustrated, the valve leaflet 104 is in an open position. For the various embodiments, the valve leaflet 104 can releasably joined to be held in this open position with a biodegradable adhesive 122 so that the commissure 106 does not help to prevent retrograde flow for at least a predetermined time after the valve has been implanted in a vessel of a body. As used herein, a "biodegradable adhesive" includes those materials that when exposed to a biological environment (e.g., *in vivo*) is chemically and/or physically degraded via one or more mechanisms. These mechanisms can include, but are not limited to, hydrolysis and/or enzymatic cleavage of the biodegradable material (e.g., scission of the polymer backbone).

With respect to valve 100, the biodegradable adhesive 122 can be positioned between the valve leaflet 104 and the valve frame 102 to hold at least the commissure 106 of the valve leaflet 104 in a static relationship relative the valve frame 102. For the various embodiments, the biodegradable adhesive 122 can originally be in the form of a liquid and/or a solid (including a gel) that can be used to join valve leaflet 104 to the valve frame 102. For example, the biodegradable adhesive 122 can be applied to one or both adjacent surfaces of the valve leaflet 104 and the valve frame 102, where the surfaces are brought together to join them with the biodegradable adhesive 122. Other forms for the biodegradable adhesive 122 are also possible.

For the various embodiments, the location(s) of and/or the surface area used with the biodegradable adhesive 122 to hold the valve leaflet 104 in the open position can vary from the proximal end 116 to the distal end 118 (or visa versa) and/or radially around the valve 100. For example, the biodegradable adhesive 122 can be positioned so as to hold the valve leaflet 104 at one or more discrete attachment points between the leaflet 104 and the frame 102. In an additional example, the biodegradable adhesive 122 can be positioned so as to hold at least the valve leaflet 104 completely along the distal end 114 of the valve frame 102. In other words, the biodegradable adhesive 122 can releasably join at least a portion of the valve leaflet 104 to the valve frame 102 along a peripheral edge of the valve leaflet 104 to the valve frame 102. For the various embodiments, releasably joining the portion of the peripheral edge of the valve leaflet 104 to the valve frame 102 includes releasably joining the peripheral edge in its entirety to the valve frame 102. Alternatively, releasably joining the portion of the peripheral edge of the valve leaflet 104 to the valve frame 102 can be at attachment points spaced equidistant from a longitudinally axis of the valve frame 102. For these embodiments, the biodegradable adhesive 122 can hold at least the commissure 106 of the valve leaflet 104 in the static relationship relative the valve frame 102 for the predetermined time after implantation into a lumen of a body.

For the various embodiments, the biodegradable adhesive 122 can be positioned between an outer surface (opposite the luminal surface) of the valve leaflet 104 and the frame member 108. In addition, the biodegradable adhesive 122 can be located over essentially the entire outer surface of the valve leaflet 104 so as to allow the biodegradable adhesive 122 to span the openings defined by the frame member 108.

For the various embodiments, the concentration(s), type, and/or mixture (e.g., two or more different biodegradable adhesives along with other optional substances) of the biodegradable adhesive 122 being used to hold the valve leaflet 104 in the open position can be varied as well. As use herein, the term "concentration" includes the amount of each of the biodegradable adhesives (e.g., by weight) in the mixture and/or solution forming the adhesive.

For the various embodiments, the selection of one or more biodegradable adhesives, their concentration and/or their location used in holding the valve leaflet 104 static relative the valve frame 102 can allow the valve leaflet 104 to release from

the valve frame in a number of ways. For example, the biodegradable adhesives 122 can be used in such a way as to allow for a progressive release of the valve leaflet 104 from one of the proximal end 112 and/or the distal end 114 of the valve frame 102. In one approach, this might be accomplished by changing the concentration and/or
5 having a gradient of the biodegradable adhesive(s) 122 that extends from the one or both of either the proximal end 112 and/or the distal end 114 of the valve frame 102.

Alternatively, the selection of one or more biodegradable adhesives 122, their concentration and/or their location can be used in such a way as to allow for each of the valve leaflets 104 to be release from their static relationship in essentially their
10 entirety at essentially the same time. For example, different types of the biodegradable adhesives 122 can be used in different regions (e.g., discrete regions) so as to allow for the progressive release of the valve leaflet 104.

For the various embodiments, the type of biodegradable adhesives can include, but are not limited to those compounds that erode (e.g., bioerodible or biodegradable)
15 so as to be absorbed by the body. As used herein, "erode" or "erosion" includes processes by which a material that is insoluble in water is converted into one that is water-soluble. Other types of biodegradable adhesives can include a variety of natural, synthetic, and biosynthetic polymers that are biodegradable, such as those having at least a heteroatom-containing polymer backbone. Such biodegradable
20 adhesives can include those having chemical linkages such as anhydride, ester, or amide bonds, among others. These chemical linkages can then undergo degradation through one or both of hydrolysis and/or enzymatic cleavage resulting in a scission of the polymer backbone.

Examples of biodegradable adhesives 122 are those that include poly(esters)
25 based on polylactide (PLA), polyglycolide (PGA), polycaprolactone (PCL), and copolymers thereof. Other biodegradable adhesives 122 can include those that having poly(hydroxyalkanoate)s of the PHB-PHV class, additional poly(ester)s, and natural polymers, such as modified poly(saccharide)s, e.g., starch, cellulose, and chitosan, which upon further hydrolysis can yield low molecular weight oligosaccharides.
30 Poly(ethylene oxide), PEO, and/or poly(ethylene glycol), PEG, can also be used as the biodegradable adhesive. Multiblock copolymers of poly(ethylene oxide) (PEO) and poly(butylene terephthalate) (PBT) are also possible for use in the biodegradable adhesives of the present disclosure, where the degradation rate can be influenced by PEO molecular weight and content.

For the various embodiments, the biodegradable adhesive 122 can hold at least the commissure 106 of the valve leaflet 104 in the static relationship relative the valve frame 102 for a predetermined time after implantation into a lumen of a body. For the various embodiments, the predetermined time after implantation can be a range of approximate time, as the degradation of the biodegradable adhesive 122 will most likely proceed at a different rate for each individual patient. As such, the type(s), concentration(s), and/or location(s) of the biodegradable adhesive 122 used in any particular valve 100 may be patient specific and/or implant location specific.

For example, the biodegradable adhesive 122 can hold at least a portion of the valve leaflet 104 static relative the valve frame 102 for no less than one week (i.e., 7 days). After this predetermined time the biodegradable adhesive 122 can have degraded and/or eroded to a point that the biodegradable adhesive 122 no longer can hold the at least a portion of the valve leaflet 104 static relative the valve frame 102. The valve leaflet 104 can then be released from the portions of the valve frame 102 with the biodegradable adhesive 122. After being released, the valve leaflet 104 can then operate to control the flow of a fluid (e.g., blood) through the valve in an essentially unidirectional manner.

For the various embodiments, the predetermined time also allows the valve frame 102 to be at least be partially in-grown at the implant site (e.g., anchor) before exposing the valve 100 to forces imparted through the opening and closing of the valve leaflet 104. In one embodiment, the valve frame 102 can have one or more of a surface treatment and/or a coating that promotes and/or discourages in-growth and/or overgrowth of the surrounding tissues. For example, the valve frame 102 can have one or more of the surface treatment and/or the coating that promotes tissue in-growth in regions of the valve 100 where the valve leaflet 104 was not attached to the valve frame 102 with the biodegradable adhesive 122. Similarly, the regions where the biodegradable adhesive 122 joints the valve leaflet 104 and the valve frame 102 can include one or more of the surface treatment and/or the coating that discourages in-growth and/or overgrowth of the surrounding tissues at least for the time it takes for the biodegradable adhesive 122 to degrade and/or erode.

For the various embodiments, the biodegradable adhesive 122 and/or the valve frame 102 can also have a predetermined structure and/or shape that allows for tissue in-growth of the valve 100, while preventing in-growth around the valve leaflet 104 while it is in its static relationship to the valve frame 102. For example, the

biodegradable adhesive 122 positioned between the valve leaflet 104 and the valve frame 102 can have a portion or a layer with a porosity that promotes and/or allows for tissue in-growth, while an adjacent portion of the biodegradable adhesive 122 may not be designed to promote such in-growth. In other words, the biodegradable adhesive 122 can have a layered structure in which the different layers and/or regions can potentially promote different in-growth responses from the body due the physical structure and/or morphology of the biodegradable adhesive 122. Alternatively, different types of biodegradable adhesives 122 can be used in either layers and/or patterns having the same and/or different morphology (e.g., structure such as porous) in trying to elicit the in-growth response discussed herein.

In some embodiments, the frame members 108 of the valve frame 102 can be formed of a variety of materials. Such materials include, but are not limited to, metals, metal alloys, and/or polymers. The design and configuration of the valve frame 102 can be such that it is balloon expandable, either fully or at least partially, and/or self expanding shape-memory materials. Examples of shape-memory materials include shape memory plastics, polymers, thermoplastic materials, and metal-alloys which are inert in the body. Some shape-memory materials, (e.g., nickel-titanium alloys) can be temperature-sensitive and change shape at a designated temperature or temperature range. In one embodiment, the shape memory metal-alloy includes those made from nickel and titanium in specific ratios, commonly known as Nitinol. Other materials are also possible.

For the various embodiments, the frame members 102 can have similar and/or different cross-sectional geometries along their length. The similarity and/or the differences in the cross-sectional geometries can be selected based on one or more desired functions to be elicited from each portion of the valve frame 102. Examples of cross-sectional geometries include rectangular, non-planar configuration (e.g., bent), round (e.g., circular, oval, and/or elliptical), polygonal, arced, and tubular. Other cross-sectional geometries are possible.

The valve 100 can further include one or more radiopaque markers (e.g., tabs, sleeves, welds). For example, one or more portions of the valve frame 102 can be formed from a radiopaque material. Radiopaque markers can be attached to and/or coated onto one or more locations along the valve frame 102. Examples of radiopaque material include, but are not limited to, gold, tantalum, and platinum. The position of the one or more radiopaque markers can be selected so as to provide

information on the position, location, and orientation of the valve 100 during its implantation.

The valve 100 further includes the valve leaflets 104 having surfaces defining a reversibly sealable opening (e.g., the commissure 106) for unidirectional flow of a liquid through the valve 100. Each of the valve leaflets 104 are coupled to the valve frame 102, where the leaflets 104 can repeatedly move between an open state and a closed state for unidirectional flow of a liquid through a lumen of the valve 100 after the biodegradable adhesive 122 has degraded and/or eroded to the point where the valve leaflets 104 are released from their static relationship with the valve frame 102. In the present example, the valve 100 includes two of the valve leaflets 104 for a bi-leaflet configuration. As appreciated, mono-leaflet, tri-leaflet and/or other multi-leaflet configurations are also possible.

In some embodiments, the leaflets 104 can be derived from autologous, allogeneic or xenograft material. As will be appreciated, sources for xenograft material (e.g., cardiac valves) include, but are not limited to, mammalian sources such as porcine, equine, and sheep. Additional biologic materials from which to form the valve leaflets 104 include, but are not limited to, explanted veins, pericardium, fascia lata, harvested cardiac valves, bladder, vein wall, various collagen types, elastin, intestinal submucosa, and decellularized basement membrane materials, such as small intestine submucosa (SIS), amniotic tissue, or umbilical vein.

Alternatively, the leaflets 104 can be formed from a synthetic material. Possible synthetic materials include, but are not limited to, expanded polytetrafluoroethylene (ePTFE), polytetrafluoroethylene (PTFE), polystyrene-polyisobutylene-polystyrene (SIBS), polyurethane, segmented poly(carbonate-urethane), polyester, polyethylene (PE), polyethylene terephthalate (PET), silk, urethane, Rayon, Silicone, or the like. In an additional embodiment, the synthetic material can also include metals, such as stainless steel (e.g., 316L) and Nitinol. These synthetic materials can be in a woven, a knit, a cast or other known physical fluid-impermeable or permeable configurations. In addition, gold plated metals can be embedded in the leaflet 104 material (e.g., a sandwich configuration) to allow for visualization of the leaflets 104 post placement.

As will be appreciated, the valve 100 (e.g., valve frame 102 and/or valve leaflets 104) can be treated and/or coated with any number of surface or material treatments. Examples of such treatments include, but are not limited to, bioactive

agents, including those that modulate thrombosis, those that encourage cellular in-growth, through-growth, and endothelialization, those that resist infection, anti-thrombogenic coatings, and those that reduce calcification. One example of a suitable coating for at least the valve frame 102 is a stent frame coating provided
5 under the trade designator Taxus® from Boston Scientific.

Referring now to Figures 2A-2B, there is illustrated different embodiments of a system 230 according to the present disclosure. For each system 230, there is at least a valve 200, as described herein, positioned at least partially over an elongate delivery catheter 232. As illustrated, the elongate delivery catheter 232 can include a
10 guide wire lumen 234 for receiving and passing a guide wire 236.

The embodiment of the system 230 illustrated in Figure 2A further includes an expandable balloon 238 positioned around at least a portion of the elongate delivery catheter 232, and where the valve 200 is positioned at least partially over the expandable balloon 238. For this embodiment, the elongate delivery catheter 232
15 further includes an inflation lumen 240 that extends through the elongate delivery catheter 232 from an inflation port 242 to an expandable volume defined at least in part by the expandable balloon 238 and the elongate delivery catheter 232. Fluid delivered under pressure through the inflation port 242 can then be used to inflate the expandable balloon 238 thereby at least partially, or completely, delivering the valve
20 200 to the desired location.

In some embodiments, the expandable balloon 238 can be a perfusion balloon. A perfusion balloon can be used to radially expand the valve frame of the valve 200 while allowing fluid, for example, blood, to pass through the delivery catheter 232 and valve 200 while the valve 200 is being positioned in the vasculature.

25 In an alternative embodiment, Figure 2B provides an illustration of a system 230 that includes a retractable sheath 250 positioned around at least a portion of the elongate delivery catheter 232. In addition, at least a portion of the valve 200 can be positioned between the elongate delivery catheter 232 and the retractable sheath 250 to hold the valve 200 in a delivery state. For example, Figure 2B illustrates an
30 embodiment in which the retractable sheath 250 is positioned around at least a portion of the delivery catheter 232 to releasably hold the valve 200 in its compressed delivery (i.e., undelivered) state. The retractable sheath 250 can be retracted to allow the valve 200 to radially expand from the elongate delivery catheter 232, where the

valve frame 202 is formed at least partially from a shape memory material such as Nitinol.

Alternatively, the valve frame 202 can be formed of a material with a spring bias, where the valve 200 can expand when the sheath 250 has been removed.

5 Examples of materials with a spring bias can include, but are not limited to, medical grade stainless steel (e.g., 316L), titanium, tantalum, platinum alloys, niobium alloys, cobalt alloys, alginate, or combinations thereof.

10 In one embodiment, the retractable sheath 250 can extend co-axially with the elongate delivery catheter 232, where the sheath 250 can be moved longitudinally (e.g., slide) relative the elongate delivery catheter 232 to allow the valve 200 to radially expand from its delivery state to its deployed state. In some embodiments, moving the retractable sheath 250 relative the delivery catheter 232 can be accomplished by pulling a proximal end 256 of the sheath 250 relative a proximal end 258 of the delivery catheter 232.

15 As illustrated in Figures 2A and 2B, the valve 200 also illustrated an embodiment of the present disclosure in which the biodegradable adhesive can be used to hold the valve leaflet 204 at one or more discrete attachment points 254 to the valve frame 202. As illustrated, the portions of the peripheral edge of the valve leaflet can be releasably joined to the valve frame at attachment points spaced equidistant from a longitudinally axis 260 of the valve frame.

20 In the compressed state, as illustrated in Figures 2A and 2B, attaching the valve leaflet 204 at the one or more discrete attachment points 254 to the valve frame 202 allows at least a portion of the commissure 206 of the valve leaflet 204 to gather toward the longitudinal axis 260 when the valve frame 202 is in a radially compressed state around either the expandable balloon 238 or compressed between the retractable sheath 250 and the elongate catheter 232.

25 In additional embodiment, the system can include both an expandable balloon positioned around at least a portion of the elongate delivery catheter and a retractable sheath. The valve frame can be at least partially self-expanding (or completely self-expanding), where retracting the sheath allows the valve to expand from its delivery state towards its deployed state. The expandable balloon can then be used to fully deploy, secure, and/or more fully seat the valve frame at the desired implant location.

Each of the delivery catheter 232 and/or the retractable sheath 250 can be formed of a number of materials. Materials include polymers, such as PVC, PE,

POC, PET, polyamide, mixtures, and block co-polymers thereof. In addition, each of the delivery catheter 232 and/or the retractable sheath 250 can have a wall thickness and an inner diameter sufficient to allow the structures to slide longitudinally relative each other, as described herein, and to maintain the valve 200 in a delivery state, as
5 discussed herein.

In an additional embodiment, the valve 200 of the present disclosure can include anchoring members attached to the valve frame or frame members. Anchoring members can include barbs, hooks, etc.

For the various embodiments, the valve of the present disclosure may be used
10 with a patient that has been diagnosed with certain forms of heart failure, such as those having an essentially normal ejection fraction, but displaying signs and symptoms of heart failure. For example, in dealing with left ventricular (LV) diastolic dysfunction, improving left atrial (LA) systole can aid in the filling of a stiff LV (although not completely due to retrograde blood flow back into the pulmonary
15 venous circulation). The valve of the present disclosure may help to improve the LA systolic contribution to LV diastolic filling when implanted at the junction where the pulmonary veins and the LA meet. Potentially, these valves will help improve the work done by the LA systole in moving a much greater percentage of blood forward into the LV during diastole.

20 In addition, positioning the system having the valve as discussed herein includes introducing the system into the cardiovascular system of the patient using minimally invasive percutaneous, transluminal techniques. For example, a guidewire can be positioned within the cardiovascular system of a patient that includes the predetermined location. The system of the present disclosure, including the valve as
25 described herein, can be positioned over the guidewire and the system advanced so as to position the valve at or adjacent the predetermined location. In one embodiment, radiopaque markers on the catheter and/or the valve, as described herein, can be used to help locate and position the valve.

The valve can be deployed from the system at the predetermined location in
30 any number of ways, as described herein. In one embodiment, valve of the present disclosure can be deployed and placed in any number of cardiovascular locations. For example, valve can be deployed and placed within an artery and/or vein (e.g., a pulmonary vein) of a patient. In one embodiment, arteries and/or veins of a patient include those of the peripheral vasculature and/or the cardiac vasculature. For

example, delivery of one or more of the valves of the present disclosure to the pulmonary veins can be accomplished through transseptal puncture from the right atria into the left atria. In addition, embodiments of the valve have the potential to be used in a number of different vessels (e.g., urinary and/or lymph) where more stringent control over fluid movement is desired. Other locations are also possible.

Delivery of the valve can be accomplished through a number of different implant techniques. For example, the valve of the present disclosure can be implanted through the use of percutaneous delivery techniques, where the valve can be positioned at a predetermined location with the delivery catheter, as discussed herein.

The valve can then be deployed from the delivery catheter at the predetermined location. The catheter can then be removed from the predetermined location.

The valve, once implanted, maintains its open luminal configuration in which the proximal end portion and the distal end portion of the valve leaflet are retained in a static relationship relative the valve frame after removal of the delivery catheter. In other words, the valve leaflet(s) are held in their "open" position through the use of the biodegradable adhesive, as discussed herein. Once implanted, the biodegradable adhesive is exposed to body fluids (e.g., blood) that cause its degradation and/or erosion to the point after the predetermined time where the valve leaflet(s) is released from its static relationship relative the valve frame.

During the predetermined time, however, the open luminal configuration allows for uncontrolled blood flow through the valve. Retaining the valve leaflets to create this open luminal configuration allows longitudinal shear stresses on the valve frame to be minimized during the predetermined time, as the valve leaflets are not opening and closing to provide for unidirectional flow through the valve. During this predetermined time, tissue in-growth can occur around the valve frame. This tissue in-growth can be promoted during the predetermined time through the use of coatings and/or surface treatments, such as those discussed herein.

While the present disclosure has been shown and described in detail above, it will be clear to the person skilled in the art that changes and modifications may be made without departing from the spirit and scope of the disclosure. As such, that which is set forth in the foregoing description and accompanying drawings is offered by way of illustration only and not as a limitation. The actual scope of the disclosure is intended to be defined by the following claims, along with the full range of equivalents to which such claims are entitled. In addition, one of ordinary skill in the

art will appreciate upon reading and understanding this disclosure that other variations for the disclosure described herein can be included within the scope of the present disclosure.

5 In the foregoing Detailed Description, various features are grouped together in several embodiments for the purpose of streamlining the disclosure. This method of disclosure is not to be interpreted as reflecting an intention that the embodiments of the disclosure require more features than are expressly recited in each claim. Rather, as the following claims reflect, inventive subject matter lies in less than all features of a single disclosed embodiment. Thus, the following claims are hereby incorporated
10 into the Detailed Description, with each claim standing on its own as a separate embodiment.

What is claimed:

1. A valve (100, 200), comprising:
a valve frame (102, 202);
a valve frame (104, 204) coupled to the valve frame (102, 202), where the valve frame (104, 204) includes a commissure (106, 206) that can reversibly seal for unidirectional flow of a liquid through the valve (100, 200); and
a biodegradable adhesive (122) between the valve frame (104, 204) and the valve frame (102, 202) to hold at least the commissure (106, 206) of the valve frame (104, 204) in a static relationship relative the valve frame (102, 202).
2. The valve (100, 200) of any of the preceding claims, where the biodegradable adhesive (122) holds the valve frame (104, 204) at one or more discrete attachment points (254) to hold each valve frame (104, 204) in the static relationship relative the valve frame (102, 202).
3. The valve (100, 200) of any of the preceding claims, where the valve frame (102, 202) includes a distal end (114) and where the biodegradable adhesive (122) holds the valve frame (104, 204) completely along the distal end (114) of the valve frame (102, 202).
4. The valve (100, 200) of any of the preceding claims, where the biodegradable adhesive (122) holds at least the commissure (106, 206) of the valve frame (104, 204) in the static relationship relative the valve frame (102, 202) for a predetermined time after implantation into a lumen of a body.
5. The valve (100, 200) of any of the preceding claims, further including allowing at least a portion of the commissure (106, 206) of the valve frame (104, 204) to gather toward the longitudinal axis (260) when the valve frame (102, 202) is in a radially compressed state.
6. The valve (100, 200) of any of the preceding claims, where the valve frame (104, 204) includes an anti-thromobogenic coating.

7. The valve (100, 200) of any of the preceding claims, where the biodegradable adhesive (122) holds at least a portion of the valve frame (104, 204) static relative the valve frame (102, 202) once in vivo for a predetermined time of no less than one week.
8. A valve (100, 200), comprising:
a valve frame (102, 202);
a valve frame (104, 204) coupled to the valve frame (102, 202), where the valve frame (104, 204) includes a commissure (106, 206) that can reversibly seal for unidirectional flow of a liquid through the valve (100, 200) and an anti-thromobogenic coating; and
a biodegradable adhesive (122) between the valve frame (104, 204) and the valve frame (102, 202) to hold at least the commissure (106, 206) of the valve frame (104, 204) in a static relationship relative the valve frame (102, 202) for a predetermined time of no less than one week after implantation into a lumen of a body.
9. A system, comprising:
an elongate delivery catheter (232) (232); and
a valve (100, 200) positioned at least partially over the elongate delivery catheter (232) (232), where the valve (100, 200) includes:
a valve frame (102, 202) having frame members defining a lumen;
a valve frame (104, 204) attached to a portion of the valve frame (102, 202), the valve frame (104, 204) having a commissure (106, 206); and
a biodegradable adhesive (122) between the valve frame (104, 204) and the valve frame (102, 202) to hold at least the commissure (106, 206) of the valve frame (104, 204) in a static relationship relative the valve frame (102, 202).
10. The system of any of the preceding claims, where the elongate delivery catheter (232) (232) includes an expandable balloon (238) positioned around at least a portion of the elongate delivery catheter (232) (232), and where the valve (100, 200) is positioned at least partially over the expandable balloon (238).

11. The system of any of the preceding claims, where the elongate delivery catheter (232) (232) includes a retractable sheath (250) positioned over at least a portion of the valve (100, 200), where the retractable sheath (250) can be retracted to release the valve (100, 200) from the elongate delivery catheter (232) (232).
12. The system of any of the preceding claims, where the biodegradable adhesive (122) holds the valve frame (104, 204) at one or more discrete attachment points (254) to the valve frame (102, 202).
13. The system of any of the preceding claims, where the valve frame (102, 202) includes a distal end (114) and where the biodegradable adhesive (122) holds the valve frame (104, 204) completely along the distal end (114) of the valve frame (102, 202).
14. A method, comprising:
forming a valve (100, 200) with a valve frame (102, 202) and a valve frame (104, 204) having a commissure (106, 206); and
releasably joining at least a portion of the valve frame (104, 204) to the valve frame (102, 202) with a biodegradable adhesive (122) so the commissure (106, 206) does not help to prevent retrograde flow for at least a predetermined time after the valve (100, 200) has been implanted in a vessel of a body.
15. The method of any of the preceding claims, where releasably joining at least a portion of the valve frame (104, 204) to the valve frame (102, 202) includes releasably joining at least a portion of a peripheral edge of the valve frame (104, 204) to the valve frame (102, 202).
16. The method of any of the preceding claims, where the releasably joining the portion of the peripheral edge of the valve frame (104, 204) to the valve frame (102, 202) includes releasably joining the peripheral edge and the valve frame (102, 202) at attachment points (254) spaced equidistant from a longitudinal axis (260) of the valve frame (102, 202).

17. The method of any of the preceding claims, further including allowing at least a portion of the peripheral edge of the valve frame (104, 204) to gather toward the longitudinal axis (260) when the valve frame (102, 202) is in a radially compressed state.

18. The method of any of the preceding claims, where releasably joining the portion of the peripheral edge of the valve frame (104, 204) to the valve frame (102, 202) includes releasably joining the peripheral edge in its entirety to the valve frame (102, 202).

19. The method of any of the preceding claims, including at least partially coating the valve frame (102, 202) with a coating that promotes at least tissue in-growth; and at least partially coating the valve frame (104, 204) with an anti-thrombogenic coating.

20. A method, comprising:

positioning a valve (100, 200) at a predetermined location with a delivery catheter (232), the valve (100, 200) including a valve frame (104, 204) having a proximal end (112) portion and a distal end (114) portion relative the proximal end (112) portion, and a valve frame (102, 202);

deploying the valve (100, 200) with the delivery catheter (232) at the predetermined location;

removing the delivery catheter (232) from the predetermined location;

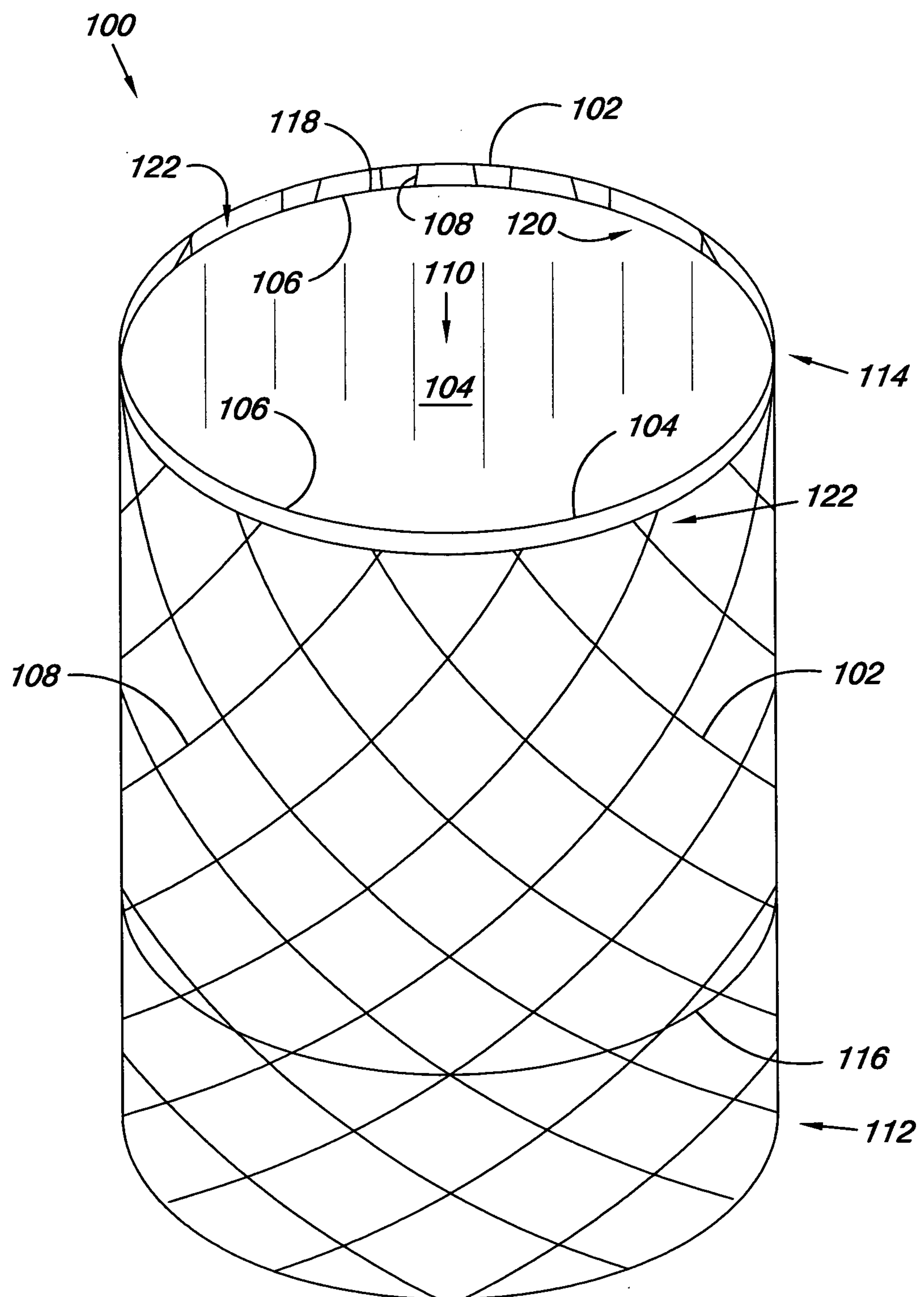
retaining the proximal end (112) portion and the distal end (114) portion of the valve frame (104, 204) in a static relationship relative the valve frame (102, 202) after removal of the delivery catheter (232) to allow for uncontrolled blood flow through the valve (100, 200); and

allowing the valve frame (104, 204) to release from its static relationship after a predetermined time.

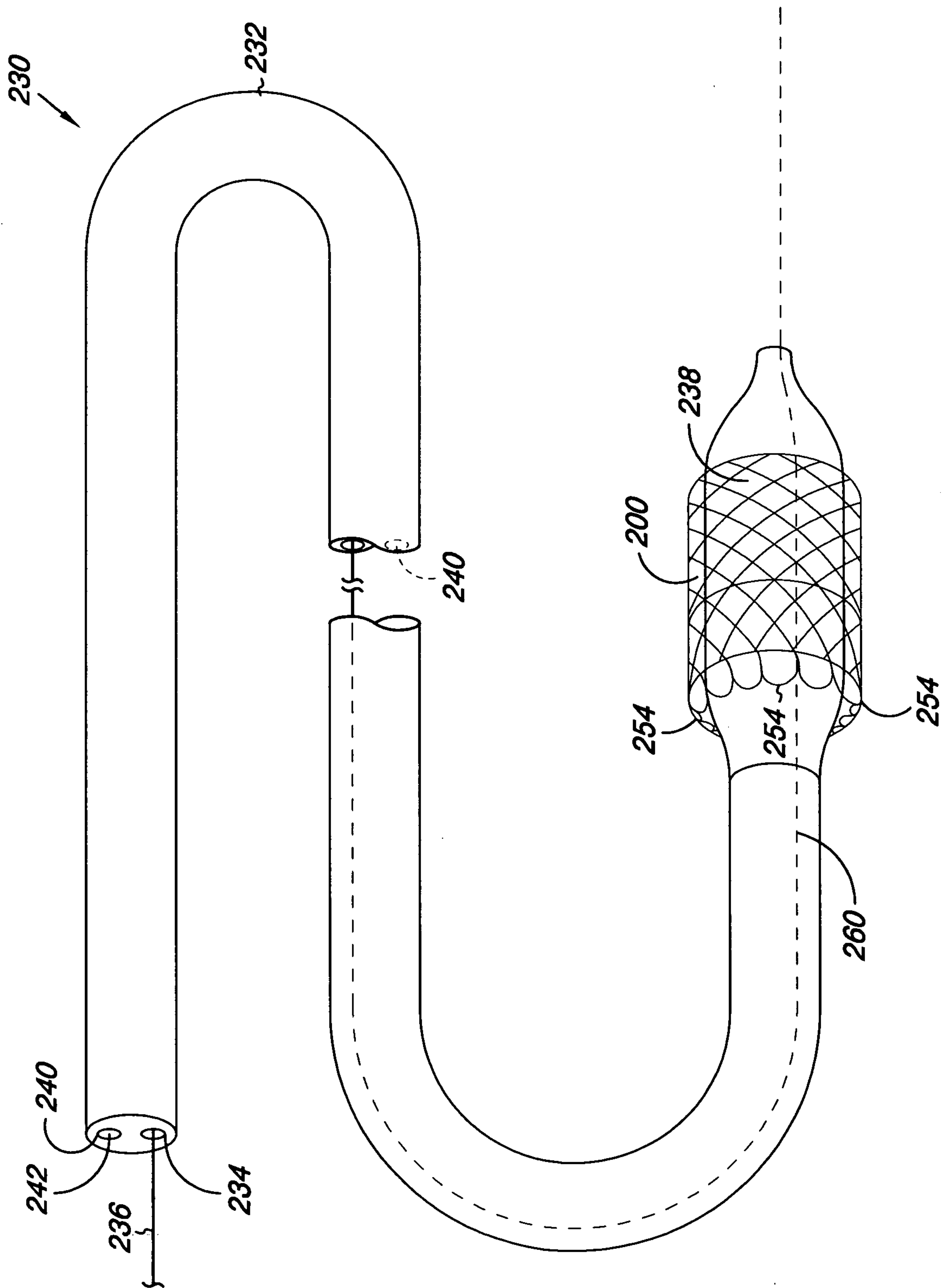
21. The method of any of the preceding claims, where positioning the valve (100, 200) at the predetermined location includes positioning the valve (100, 200) in a pulmonary vein.

22. The method of any of the preceding claims, where retaining the valve frame (104, 204) includes keeping a biodegradable adhesive (122) at least partially between the valve frame (104, 204) and the valve frame (102, 202) for a time interval of no less than one week.
23. The method of any of the preceding claims, where allowing the valve frame (104, 204) to release from its static relationship includes exposing the biodegradable adhesive (122) to body fluids that cause the biodegradation of the biodegradable adhesive (122).
24. The method of any of the preceding claims, where retaining the valve frame (104, 204) includes minimizing longitudinal shear stresses on the valve frame (102, 202) during the predetermined time.
25. The method of any of the preceding claims, including promoting tissue in-growth around the valve frame (102, 202) during the predetermined time.

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*Fig. 1*

2/3

*Fig. 2A*

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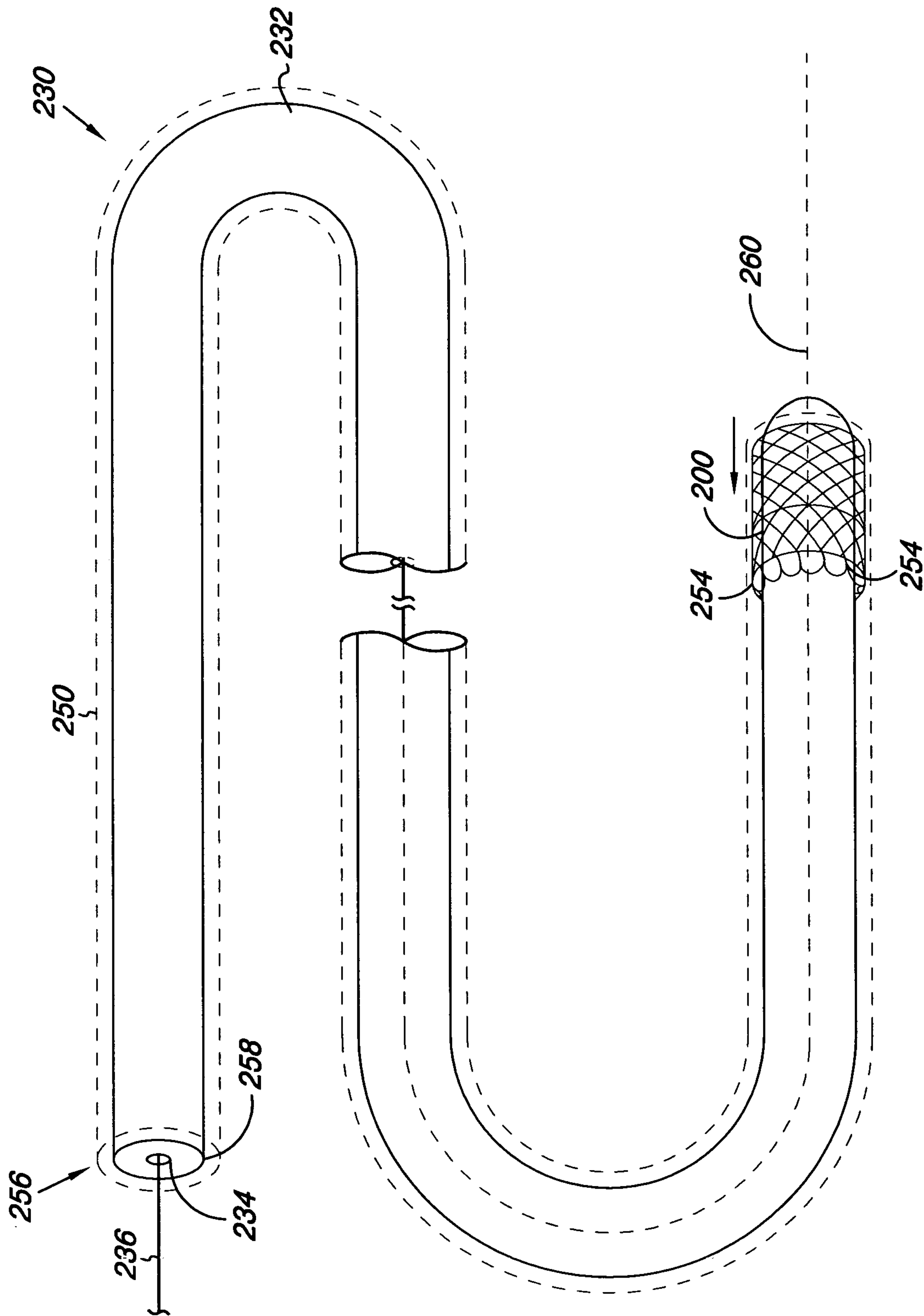
*Fig. 2B*

Fig. 1

