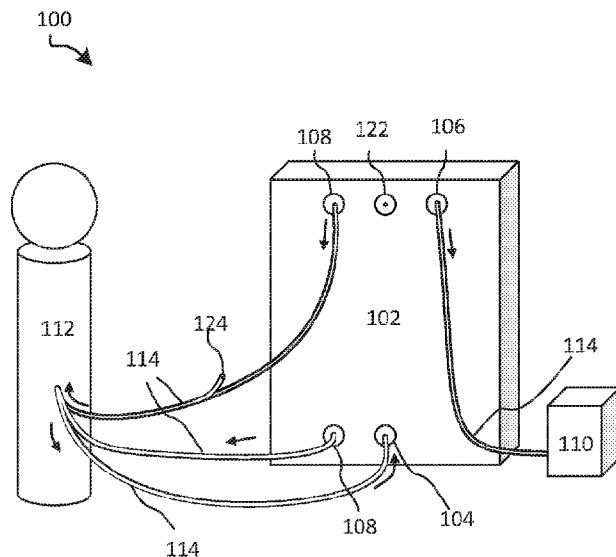




(86) Date de dépôt PCT/PCT Filing Date: 2016/06/09  
 (87) Date publication PCT/PCT Publication Date: 2017/02/09  
 (45) Date de délivrance/Issue Date: 2020/11/17  
 (85) Entrée phase nationale/National Entry: 2018/02/02  
 (86) N° demande PCT/PCT Application No.: US 2016/036626  
 (87) N° publication PCT/PCT Publication No.: 2017/023419  
 (30) Priorité/Priority: 2015/08/05 (US62/201,287)

(51) Cl.Int./Int.Cl. *A61M 1/00* (2006.01),  
*B01D 37/00* (2006.01), *B01D 37/04* (2006.01),  
*B01D 61/00* (2006.01), *B01D 61/14* (2006.01),  
*B01D 61/58* (2006.01)  
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(54) Titre : SYSTEME DE FILTRATION A FLUX TANGENTIEL POUR LA FILTRATION DE MATERIAUX PROVENANT DE FLUIDES BIOLOGIQUES  
 (54) Title: TANGENTIAL FLOW FILTER SYSTEM FOR THE FILTRATION OF MATERIALS FROM BIOLOGIC FLUIDS



(57) **Abrégé/Abstract:**

Systems and methods for filtering materials from biologic fluids are discussed. Embodiments may be used to filter cerebrospinal fluid (CSF) from a human or animal subject. The method may include the steps of withdrawing fluid comprising CSF, filtering the volume into permeate and retentate by passing the fluid through a tangential flow filter, and returning the permeate to the subject. During operation of the system, various parameters may be modified, such as flow rate.

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization  
International Bureau

(43) International Publication Date  
9 February 2017 (09.02.2017)



(10) International Publication Number  
**WO 2017/023419 A1**

(51) International Patent Classification:

*A61M 1/00* (2006.01) *B01D 61/00* (2006.01)  
*B01D 37/00* (2006.01) *B01D 61/14* (2006.01)  
*B01D 37/04* (2006.01) *B01D 61/58* (2006.01)

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(21) International Application Number:

PCT/US2016/036626

(81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY, BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IR, IS, JP, KE, KG, KN, KP, KR, KZ, LA, LC, LK, LR, LS, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SA, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

(22) International Filing Date:

9 June 2016 (09.06.2016)

(25) Filing Language:

English

(26) Publication Language:

English

(30) Priority Data:

62/201,287 5 August 2015 (05.08.2015) US

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(84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LR, LS, MW, MZ, NA, RW, SD, SL, ST, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, RU, TJ, TM), European (AL, AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV, MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK,

[Continued on next page]

(54) Title: TANGENTIAL FLOW FILTER SYSTEM FOR THE FILTRATION OF MATERIALS FROM BIOLOGIC FLUIDS

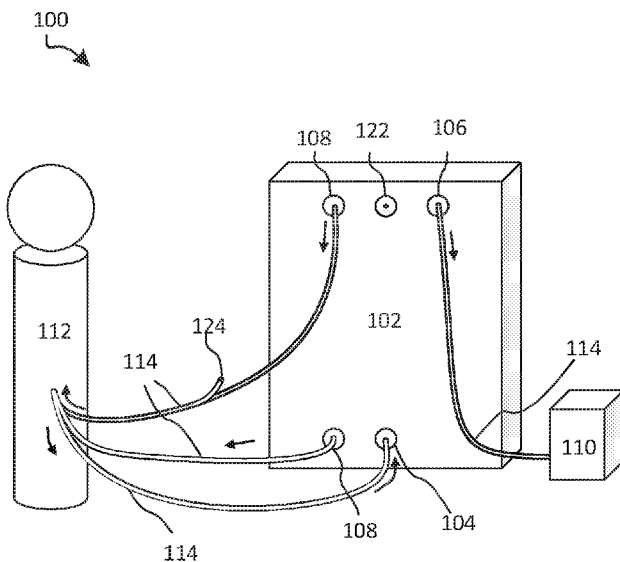


FIG. 1

(57) Abstract: Systems and methods for filtering materials from biologic fluids are discussed. Embodiments may be used to filter cerebrospinal fluid (CSF) from a human or animal subject. The method may include the steps of withdrawing fluid comprising CSF, filtering the volume into permeate and retentate by passing the fluid through a tangential flow filter, and returning the permeate to the subject. During operation of the system, various parameters may be modified, such as flow rate.

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**WO 2017/023419 A1** 

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SM, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, — *with amended claims (Art. 19(1))*  
GW, KM, ML, MR, NE, SN, TD, TG).

**Published:**

— *with international search report (Art. 21(3))*

**TANGENTIAL FLOW FILTER SYSTEM FOR THE FILTRATION OF  
MATERIALS FROM BIOLOGIC FLUIDS**

**CROSS-REFERENCE TO RELATED APPLICATIONS**

5           This application claims the benefit of the earlier filing date  
of U.S. Provisional Application Number 62/201,287, filed August 5, 2015, entitled  
“Tangential Flow Filter System for the Filtration of Materials from Biologic Fluids.”

          Embodiments described in this application may be used in combination or  
conjunction, or otherwise, with the subject matter described in one or more of the  
10 following:

          U.S. Patent Application Number 14/743,652, filed June 18, 2015, entitled  
“Devices and Systems for Access and Navigation of Cerebrospinal Fluid Space,” which  
claims priority to U.S. Provisional Application Number 62/038,998, filed August 19,  
2014; and

15           U.S. Patent Application Number 13/801,215, filed March 13, 2013, entitled  
“Cerebrospinal Fluid Purification System,” a continuation of U.S. Patent Application  
Serial Number 12/444,581, filed Jul. 1, 2010, which is the U.S. National Phase entry of  
International Patent Application Number PCT/US2007/080834, filed Oct. 9, 2007, which  
claims the benefit of U.S. Provisional Application Number 60/828,745, filed on Oct. 9,  
20 2006.

**BACKGROUND**

          A variety of diseases and conditions may be treated by filtering particular  
materials from biologic fluids. The most common filters for removing materials from  
biologic fluids are dead-end (common syringe filters), depth filters and affinity filters.  
25 Although dead-end and depth filters are easy to use and come in many pore sizes, their  
small surface area prevents them from being used for larger volumes or when trying to  
remove a significant amount of material. These filters may quickly clog because the  
mechanism of filtration deposits the material on the surface of the filter. In addition, the  
filtration of biologic materials, such as blood, may cause the material to be lysed when

- 5 filtered through dead-end filters. There exists a need in the art for improved systems and methods for filtering biologic fluids.

#### SUMMARY

According to certain embodiments, a method for filtering materials from cerebrospinal fluid (CSF) of a human or animal subject, may comprise withdrawing a  
10 volume of fluid comprising CSF from a CSF-containing space of the subject at a first flow rate using a filtration system, the filtration system operating according to a set of parameters; filtering the volume of fluid into permeate and retentate using a tangential flow filter of the filtration system; measuring a characteristic of the fluid using a sensor of the filtration system; returning the permeate to the CSF-space of the subject at a  
15 second flow rate; and updating a parameter of the set of operation parameters based on the measured characteristic responsive to determining the measured characteristic passes a predetermined threshold.

In certain implementations, the first filtration system may be in fluid connection with the CSF-containing space of the subject via a multi-lumen catheter inserted at least  
20 partially within the space. The parameter may comprise the first flow rate and the second flow rate. Updating the parameter of the set of operation parameters may comprise updating the parameter such that the first flow rate and the second flow rate are substantially the same. The characteristic may be a total volume of fluid withdrawn minus a total volume of fluid returned. The threshold may be a volume of removed CSF  
25 that is predicted to induce a spinal headache. The parameter may comprise a flow rate parameter and updating the parameter causes the first and second flow rate to decrease. The volume of removed CSF that is predicted to induce a spinal headache in a human subject may be more than approximately 15 ml per hour, such as between approximately 35 ml per hour and approximately 45 ml per hour. The rate at which the volume of fluid  
30 is withdrawn from the CSF-containing space may be between approximately 0.04 ml per minute and approximately 30 ml per minute. The characteristic may be a ratio of permeate to retentate, the threshold may be an increase in the ratio, and updating the parameter of the set of operation parameters may comprise updating the parameter such that the first flow rate and second flow rate increase. The characteristic may be an  
35 absolute retentate flow rate, the threshold may be a range of acceptable retentate flow rates, and updating the parameter of the set of operation parameters may include updating the parameter to cause the absolute retentate flow rate to return to within the

5 range of acceptable retentate flow rates. The method may further comprise adding a therapeutic agent to the permeate prior to returning the permeate. The method may also further comprise adding a volume of artificial CSF to the permeate prior to returning the permeate.

10 According to certain embodiments, a method for filtering CSF may comprise withdrawing a volume of fluid comprising CSF from a CSF-containing space of a subject at a first flow rate using a first filtration system, the first filtration system operating according to a first set of parameters; filtering the volume of fluid into a first permeate and a first retentate using a first tangential flow filter of the first filtration system; passing the first retentate to a second filtration system in fluid connection with the first  
15 filtration system, the second filtration system operating according to a second set of parameters; filtering the first retentate into a second permeate and a second retentate using a second tangential flow filter of the second filtration system; combining the first permeate and the second permeate using a combiner to form a combined permeate; measuring characteristics of the fluid using a sensor; returning the combined permeate to  
20 the CSF-containing space of the subject at a second flow rate; and updating at least one parameter of the first set of operation parameters or the second set of operation parameters based on the measured characteristic responsive to determining the measured characteristic passes a predetermined threshold.

25 In certain implementations, passing the first retentate to a second filtration system may comprise passing the retentate through a flow regulator, which regulates a flow characteristic of the second retentate. The combiner may regulate the return of the combined permeate to the CSF-containing space of the subject. The first and second flow rates may be substantially the same.

30 According to certain embodiments, a method for filtering CSF of a human or animal subject, may comprise introducing a multi-lumen catheter into a CSF-containing space of the subject, the catheter having a first port and a second port; withdrawing a volume of fluid comprising CSF from the CSF-containing space through the first port; filtering the volume of fluid into permeate and retentate by passing the volume of fluid through a tangential flow filter of the filtration system at a pressure and a flow rate; and  
35 returning the permeate to the CSF-containing space of the subject through the second port.

In certain implementations, the method may include increasing at least one of the pressure and the flow rate responsive to determining the ratio of permeate to retentate

has increased. Both the pressure and the flow rate may be increased responsive to determining the ratio of permeate to retentate has increased. The volume of fluid may be withdrawn at a withdrawal flow rate, the retentate may be returned at a return flow rate, and the withdrawal flow rate and the return flow rate may be substantially the same.

5                   In some embodiments, there is provided a system for filtering materials from cerebrospinal fluid (CSF) of a human or animal subject, the system comprising: a filtration system configured for withdrawing a volume of fluid comprising CSF from a CSF-containing space of the subject at a first flow rate, the filtration system configured for operating according to a set of operation parameters; a tangential flow filter configured for filtering the  
10 volume of fluid into permeate and retentate; a sensor configured for measuring a characteristic of the fluid, wherein the characteristic comprises a ratio of permeate to retentate; wherein the filtration system is configured to return the permeate to the CSF-containing space of the subject at a second flow rate; and wherein the filtration system is configured to update a parameter of the set of operation parameters based on the measured characteristic responsive  
15 to determining the measured characteristic passes a predetermined threshold, wherein updating the parameter causes the first flow rate and the second flow rate to increase.

                  In some embodiments, there is provided a system for filtering cerebrospinal fluid (CSF) of a human or animal subject, the system comprising: a multi-lumen catheter configured to be introduced into a CSF-containing space of the subject, the catheter having a  
20 first port and a second port; wherein the multi-lumen catheter is configured to withdraw a volume of fluid comprising CSF from the CSF-containing space through the first port at a withdrawal flow rate; a tangential flow filter configured for filtering the volume of fluid into permeate and retentate by passing the volume of fluid through the tangential flow filter of the system at a pressure and a filter flow rate; and wherein the multi-lumen catheter is configured  
25 to return the permeate to the CSF-containing space of the subject through the second port at a return flow rate; and wherein the system is configured to increase the withdrawal flow rate and the return flow rate responsive to determining that a ratio of permeate to retentate has increased.

#### BRIEF DESCRIPTION OF THE DRAWINGS

30                   FIG. 1 illustrates a system for the filtration of materials from biologic fluids

according to certain implementations, with solid arrows indicating an example fluid flow direction.

FIG. 2A illustrates fluid being withdrawn from and returned to a reservoir, according to certain implementations

5 FIG. 2B illustrates fluid being withdrawn from and returned to a reservoir, according to certain implementations.

FIG. 2C illustrates a block diagram of a filtration system, according to certain implementations, with solid arrows indicating an example fluid flow path and dashed arrows indicating an example flow path for signals or information.

10 FIG. 2D illustrates a section of a tangential flow filtration system according to certain implementations.

FIG. 3 illustrates a system for the filtration of materials from biologic fluids according to certain implementations, with solid arrows indicating an example fluid flow direction.

15 FIG. 4 illustrates a flow diagram for a method for using a filtration system for the filtration of materials from biologic fluids.

FIG. 5 illustrates a flow diagram for a method of controlling fluid flow within a filtration system.

#### DETAILED DESCRIPTION

20 Disclosed embodiments generally relate to systems and methods for filtering materials from biologic fluids of a human or animal subject. In certain implementations, a tangential flow filter may be used to separate cerebrospinal fluid (CSF) into permeate and retentate. The permeate may be returned to the subject. In certain implementations, the retentate may be filtered again, for example, through one or more additional tangential flow  
25 filters or through different methods of filtering. During operation of the system, various parameters may be modified, such as flow rate and pressure. Certain



5 systems and methods described herein may be combined with other systems and methods for conditioning, removing, or otherwise processing biological materials, such as those discussed in U.S. Patent No. 8,435,204.

FIG. 1 illustrates a system 100 for the filtration of materials from biologic fluids according to certain embodiments, including a filtration system 102, an intake 104, a  
10 retentate outlet 106, a permeate outlet 108, a vessel 110, a reservoir 112, and tubing 114. The arrows represent an example direction that fluid may take through the system.

In certain embodiments, the filtration system 102 is a device or combination of devices that is configured to filter, concentrate, dialyze, separate, or otherwise treat or condition the contents of a fluid. The filtration system 102 may be a tangential flow  
15 filtration system (for example, as shown and described in relation to FIG. 2) or other system configured to filter fluid. In certain embodiments, the filtration system 102 receives the fluid through the intake 104 and separates the fluid into retentate and permeate. The retentate exits the filtration system 102 through a retentate outlet 106, and the permeate exits the filtration system 102 through a permeate outlet 108.

20 The intake 104 may be a port through which fluid enters the filtration system 102. The retentate outlet 106 may be an outlet through which retentate exits the filtration system 102. The permeate outlet 108 may be an outlet through which permeate exits the filtration system 102.

The intake 104, retentate outlet 106, and permeate outlet 108 may be any kind of  
25 ports through which material or fluid may flow. These components may be configured to be in fluid connection by tubing 114. The components 104, 106, 108, 114 may include various fittings to facilitate the connection, including but not limited to compression fittings, flare fittings, bite fittings, quick connection fittings, Luer-type fittings, threaded fittings, and other components configured to enable fluid or other connection between  
30 two or more components. In addition to fittings, the components 104, 106, 108, 114 may also include various elements to facilitate use of the system 100, including but not limited to various valves, flow regulators, adapters, converters, stopcocks, reducers, and other elements.

In certain embodiments, there may be one or more permeate outlets 108 and one  
35 or more retentate outlets 106. For example, the systems 100, 300 illustrated in FIGS. 1 and 3, respectively, include a filtration system 102 having two permeate outlets 108. This configuration may facilitate the use of different filtration systems within a filtration

5 system 102, 302. For example, the filtration systems 102, 302 may include multiple filtration components, each with their own individual outlets.

The vessel 110 may be a container for storing fluid. For example, fluid leaving the filtration system 102 may be deposited in the vessel 110. The fluid deposited in the vessel 110 may be held for storage, waste disposal, processing, testing, or other uses. The  
10 vessel 110 may also be a reservoir for subsequent filtering, for example, through the same or different set of filters. This fluid may or not be combined with previously filtered fluid.

The reservoir 112 may contain a particular fluid to be filtered. In certain implementations, the reservoir 112 may be an anatomical entity or location within a  
15 human or animal subject, such as a chamber or CSF-containing space or a blood vessel. The reservoir 112 may be the source of the fluid, the destination of the fluid, or both. For example, the system 100 may remove or receive a volume of fluid from the reservoir 112, perform filtration and/or other treatment, and return a portion of the processed and/or treated fluid to the reservoir 112.

20 The various components of the system 100 may be connected through tubing 114. For instance, in certain embodiments, there may be a length of the tubing 114 placing the reservoir 112 in fluid connection with the intake 104. The permeate outlet 108 may be in fluid connection with the reservoir 112 via a length of the tubing 114. The retentate outlet 106 may be in fluid connection with the vessel 110 via a length of the tubing  
25 114. The tubing 114 may be any kind of system for transporting or containing fluid. While the connections within the system 100 are shown as being direct, the connections need not be. The various portions of the system 100 may be connected through combinations of connections and various tubing 114. In certain embodiments, the tubing 114 and other portions of the system 100 may be filled with priming fluid (e.g.,  
30 saline). Longer lengths of tubing 114 may correspondingly comprise a larger amount of priming fluid; however, in certain implementations, larger amounts of priming fluid may result in an undesirable amount of dilution of “natural” fluid, such as CSF. Accordingly, in certain implementations, the tubing 114 may be selected in order to minimize the volume of priming fluid needed, while still having the system be practically useful (e.g.,  
35 enough tubing to enable the system 100 to be used at a subject’s bedside). Depending on the subject and the reservoir 112, the tolerance for removal or dilution of fluid may vary, and the system 100 may be scaled accordingly. For example, the parameters of the

5 system 100 may be changed to scale to suit subjects ranging from a mouse to a human or larger mammal.

In certain implementations, the tubing 114 may have a port 124 to access the fluid traveling within the tubing 114. As illustrated in FIG. 1, there is a port 124 between the permeate outlet 108 and the reservoir 112. This port 124 may be configured for the introduction of additives, such as therapeutic agents, artificial fluid (such as artificial CSF), and/or other additives. The port 124 may also be configured for the removal of fluid for testing or other purposes. For example, in certain embodiments, fluid returning to the reservoir 112 may be removed and tested for particular characteristics or parameters. In certain embodiments, tubing 114 that links the reservoir 112 to the intake 104 may include a port 124. This port 124 may also be used for the introduction of additives and/or the removal of fluid. In certain implementations, instead of or in addition to a port 124 located on the tubing 114, there may also be a port 122 located on the filtration system 102 itself. This port 122 may be used to access the fluid within the filtration system 102 at various points during filtration for various purposes. For example, like the port 124, the port 122 may be used to introduce additives to the system 100 or remove fluid therefrom. In some embodiments, the ports 122, 124 may be used to link the system 100 with other systems.

FIG. 2A illustrates a system and method for withdrawing a fluid 202 from and returning fluid to the reservoir 112, according to certain implementations. The connection between the system 100 and anatomical structures (such as the reservoir 112) may be made in a variety of ways. For example, if the reservoir 112 is an anatomical location within a subject, as shown in FIG. 2A, the connection with the reservoir 112 may be made through one or more catheters inserted into particular anatomical locations. For example, the catheter may be a multi-lumen catheter inserted through a single opening in the subject to access the anatomical location or may be two catheters inserted at two different, but connected anatomical locations. In certain implementations, the connection may be made via an external ventricular drain system. For example, the tip of a catheter may be placed in a lateral ventricle of the brain.

As a specific example, the certain implementations shown in FIG. 2A include a portion of a subject's spine 200, including vertebrae 201, carrying a fluid 202 (for example, a fluid comprising CSF), and a multi-lumen catheter 204. The multi-lumen catheter 204 may comprise a first port 206 and a second port 208 that place the reservoir 112 in fluid connection with tubing 114. As illustrated, a first volume of the fluid 202

5 enters the multi-lumen catheter 204 through the first port 206 and is passed through into a portion of the tubing 114 (for example, a portion of tubing 114 leading to the intake 104). A second volume of fluid 202 enters the multi-lumen catheter 204 from a portion of the tubing 114 (for example, a portion of tubing 114 coming from the permeate outlet 108) and exits the multi-lumen catheter 204 through the second port 208.

10 FIG. 2B illustrates a system and method for withdrawing fluid from and returning fluid to the reservoir 112, according to certain implementations. In this particular example, the multi-lumen catheter 204 is placed in fluid connection with the ventricles of a subject's brain 210 in a configuration typically referred to as an external ventricular drain.

15 Although FIGS. 2A and 2B illustrate accessing CSF in a portion of the spine 200 and a portion of the brain 210, respectively, the embodiments disclosed herein need not be limited to those regions or that fluid and may be used with other locations and fluids. For example, one or more single-lumen catheters may be used to transport the fluid 202. As another example, the anatomical location may be a blood vessel and the fluid may be  
20 blood.

FIG. 2C illustrates a block diagram of a filtration system 102 according to certain embodiments, with solid arrows indicating an example flow path for fluids and materials, and dashed arrows indicating an example flow path for signals and information. FIG. 2C illustrates the intake 104, the retentate outlet 106, the permeate outlet 108, a pump 222, a  
25 sensor 224, a filter 226, a processing unit 228, and an interface 230.

The pump 222 may be any device for inducing fluid flow through one or more portions of the filtration system 102. In certain embodiments, the pump 222 may be a peristaltic pump, which may reduce the need for sterilization of complex pump components; however, other types of pumps may be used. The operation of the pump  
30 222 may be controlled by modifying the operating parameters of the pump 222. This may enable the flow rate, pressure, and/or other parameters of the pump 222 to be changed. The pump 222 may also be used to withdraw the fluid from the reservoir 112.

The sensor 224 may be a device for generating and/or receiving information, including but not limited to one or more of characteristics of the fluid withdrawn from  
35 the reservoir 112, before, after, and/or during filtration, including but not limited to temperature; pressure; the ratio of permeate volume to retentate volume; the fluid flow rate to and/or from the reservoir 112; the amount of contaminants or other materials in the fluid; the fluid flow return rate; the filter efficiency; filter status (for example,

5 whether the filters are clogged or otherwise running inefficiently); and other parameters or characteristics. While the sensor 224 is shown within the filtration system 102, one or more sensors 224 may be located elsewhere in the system 100 and/or cooperate with other locations. The sensor 224 may convert the data into computer- and/or human-readable representations for processing.

10 The filter 226 may be a device for separating a first portion of materials and/or fluid from a second portion of materials and/or fluid. The design and type of the filter 226 may vary depending on the type of fluid and the desired filtration results. For example, the filter 226 may be a tangential flow filter configured to separate the fluid into permeate and retentate (see, for example, FIG. 2D) with the retentate flowing to the retentate outlet 106 and the permeate flowing to the permeate outlet 108. For example, 15 various combinations of filters may be used to achieve different kinds of filtration. For example, the filters may include filters of various pore sizes and different attributes. For example, filtering schemes may include ultrafiltration, microfiltration, macrofiltration and other sized filters that have various porosities. Combinations of filters may include 20 dead end filtration, depth filtration, tangential flow filtration, affinity filtration, centrifugal filtration, vacuum filtration, and/or combinations thereof. Multiple filtration systems may be useful in order to continually re-filter retentate in order to yield a higher volume of permeate that may be returned to the reservoir 112.

The processing unit 228 may be a device configured to control the operation of 25 the filtration system 102, for example by sending signals to the pump 222, sensor 224, and/or filter 226. In some embodiments, the signals are sent in response to receiving input from the interface 210. In certain embodiments, the processing unit 228 may be processing information, such as data received from the sensor 224 and/or the interface 210 and making decisions based on the information. In certain embodiments, the 30 processing unit 228 may itself make decisions based on the information. For example, the processing unit 228 may include a processor and memory for running instructions configured to receive input, make decisions, and provide output.

The interface 230 may be a device or system of devices configured to receive input and/or provide output. In certain embodiments, the interface 230 is a keyboard, 35 touchpad, subject monitoring device, and/or other device configured to receive input. For example, a healthcare professional may use the interface 230 to start or stop the system 100 and to modify system parameters, such as the absolute duration of the procedure, pump speed, and other parameters. The interface 230 may also include a display,

5 speaker, or other device for sending user-detectable signals. In certain implementations, the interface 230 may comprise a network interface configured to send communications to other devices. For example, the interface 230 may enable the filtration system 102 to communicate with other filtration systems, flow control devices, a server, and/or other devices.

10 FIG. 2D illustrates a segment of the filter 226 according to certain implementations, including a first section 256, a membrane 258, and a second section 260, with arrows indicating flow direction. As shown in FIG. 2D, the filter 226 is configured as a tangential flow filter. In this configuration, the fluid 202 may enter the filter 206 and pass through the first section 256. While the fluid 262 travels through the first section 256, the fluid 262 may encounter the membrane 258. A particular pressure, flow rate, or other environmental condition within the first section 256 and/or second section 260 may draw or otherwise encourage fluid to contact the membrane 258. The environmental condition may be created by, for example, the shape, size, or configuration of the filter 226. The environment may also be created as a result of the pump 222 or other feature of the filtration system 102 or system 100. As a result, certain components of the fluid 262 (for example, components 252) may pass through an aperture of the membrane 258 to the second section 260. However, certain other components (for example, contaminants 254) may be improperly sized (for example, the certain other components are too large) to pass through the membrane 258 and instead remain within the first section 256. The fluid 262 that passes through the membrane 258 into the second section 260 may be described as the permeate and may pass through to the permeate outlet 108.

As a specific example, the fluid 262 may be CSF having particular desirable components 252. The CSF may also contain contaminants 254, such as blood cells, blood cell fragments, hemolysis components, neutrophils, eosinophils, inflammatory cells, proteins, misfolded proteins, cytokines, bacteria, fungi, viruses, small and large molecules, oligomers (such as A $\beta$  oligomers, tau oligomers,  $\alpha$ -synuclein oligomers, and Huntingtin oligomers), antibodies (such as anti-myelin antibodies), enzymes, mutated enzymes (such as mutations to SOD1), and/or other substances. The contaminants 254 may, but need not, include materials or matter that are present in CSF normally (e.g. a cytokine that is present in CSF normally but is present in an elevated or otherwise undesirable amount). One or more of the contaminants 254 may be associated with or suspected to be associated with one or more diseases or conditions. For example, the

contaminants 254 may be associated with one or more of Alzheimer's disease, Parkinson's disease, multiple sclerosis, Huntington's disease, amyotrophic lateral sclerosis, for instance, as described in U.S. Application Number 13/801,215

5 published as US Publication No. 2014/0066830. The filter

226 may be used to separate the contaminants 254 from the fluid and/or desirable components 252 of the CSF. For instance, a membrane 258 may be sized or otherwise configured to allow CSF to flow through the membrane 258 while substantially preventing contaminants 254 from passing through the membrane 258.

10 FIG. 3 illustrates a system 300 for the filtration of materials from biologic fluids according to certain embodiments. The system 300 may include additional components, such as but not limited to one or more flow (or pressure) regulators 118, 318, combiner 116, and filtration system 302 (for example, as described in reference to filtration system 102). Filtration system 302 may include an intake 304 (for example, as described above  
15 in reference to intake 104), a retentate outlet 306 (for example, as described in reference to retentate outlet 106), and a permeate outlet 308 (for example, as described above in reference to permeate outlet 108). The arrows represent flow direction.

In certain implementations, system 300 includes the filtration system 102 and, rather than having the retentate outlet 106 connected directly to the vessel 310, the  
20 retentate outlet 106 may be connected first to a flow regulator 118 and then to the intake 304 of the second filtration system 302. The permeate outlet 108 and permeate outlet 308 may be connected via a combiner 116 for flow to the reservoir 112. However, the permeate outlets 108, 308 need not necessarily be combined and may return via separate pathways to the reservoir 112. The retentate outlet 306 may be connected to the vessel  
25 310 via a flow regulator 318.

The flow regulators 118, 318 may be devices configured to regulate one or more fluid flow characteristics of the system 300. These characteristics may include but are not limited to flow rate, direction, and pressure. While the flow regulators 118, 318 are illustrated as components outside of the filtration systems 102, 302, they need not be or  
30 need only be located outside of the filtration systems 102, 302 or in the exact locations illustrated. In certain embodiments, the flow regulators 118, 318 may be located within the filtration systems 102, 302. In certain implementations, the filtration systems 102, 302 or other portions of the systems 100, 300 may include additional flow regulators. The flow regulator may include various components or subsystems for controlling flow  
35 characteristics and may include pressure regulators, backpressure regulators, sensors,

5 and/or other devices. The flow regulators may be controllable by other components of the system (e.g., processing unit 228).

The combiner 116 may be a device in which the fluid from two or more tubes 112 is combined into a single fluid flow. For example, as illustrated in FIG. 3, the combiner 116 takes in fluid from the permeate outlet 108 and the permeate outlet 308  
10 and combines the fluid into a single length of tubing 114 for deposit within the reservoir 112. In some embodiments, the combiner 116 may be a simple junction that places the flow from the outlets 108, 308 in fluid connection with the tubing 114 leading to the reservoir 112. In some embodiments, the combiner 116 may facilitate the mixing of the fluid. In certain embodiments, the combiner 116 may also include a mechanism for flow  
15 regulation. For example, the combiner 116 may smooth turbulent flow, buffer fluid for smooth deposit within the reservoir 112, remove air bubbles from the fluid, and perform other flow regulation or fluid treatment. The combiner 116 may also regulate the flow, direction, and pressure rate of the fluid being deposited within the reservoir 112.

The filtration system 302 may be a filtration system as described above in  
20 reference to filtration system 102. However, the filtration systems 102, 302 may be different. For example, the filtration system 102 may be configured to filter a particular kind of contaminant 254 while the filtration system 302 may be configured to filter a different kind of contaminant 254. In other embodiments, the filters may provide selective or progressive filtration, such as by having one set of pore sizes in filtration  
25 system 102 and then a set of smaller pore sizes in filtration system 302, such as to provide increased filtration of the same or different contaminants 254 and/or other substance or materials. One or both filtration systems 102, 302 may use tangential flow filtration, other filtration, or combinations thereof.

FIG. 4 illustrates a method 400 for using a filtration system for the filtration of  
30 materials from biologic fluids, including the steps of starting the process 402, withdrawing a volume of fluid 404, filtering and/or otherwise treating the volume of fluid 406, measuring characteristics 408, returning a volume of fluid 410, determining  
412, updating parameters 414, and ending the process 416. The method may be utilized with certain embodiments, including system 100 and system 300. While the method will  
35 be described with reference to system 300, a person of skill in the art would be able to modify the steps in order to be used with other systems, including but not limited to system 100 or various combinations of systems.



5           While the method is described as being performed on a particular volume of fluid, the system may operate on a continuous flow of fluid. That is, the system 300 need not necessarily withdraw a volume of fluid, wait for the volume to be processed and returned, and then withdraw another volume of fluid. The method may follow a continuous process. Similarly, while FIG. 4 appears to illustrate a series of consecutive  
10 steps, the steps of the described method may occur concurrently. For example, the system 300 may concurrently perform some or all of the steps illustrated in FIG. 4. For instance, the system 300 may concurrently withdraw and return fluid.

          The method 400 may begin at start 402. This step 402 may include activating one or more components of the system 300. This step 402 may also include or follow  
15 various preparation steps. Such steps may include installing filtration components, selecting and preparing the reservoir 112, installing tubing 114, calibrating components, priming components of the system 300, and other steps.

          The installing filtration components step may include selecting particular filtration components based on desired outcomes, the particular reservoir 112, fluid, or  
20 other considerations. For example, if the method 400 is being used on a subject suffering from a cerebral vasospasm, the goal of the procedure may be to filter blood breakdown products from the subject's CSF. This would make the reservoir 112 a lumen carrying CSF, the fluid. As such, particular filtration components would be selected to filter the blood components from the CSF. For example, a membrane 258 with apertures sized to  
25 substantially prevent the flow of blood components, while large enough to substantially allow the entry of CSF as permeate, may be used.

          The selecting and preparing the reservoir 112 step may include choosing a particular reservoir 112. For example, a healthcare professional may select an individual who may benefit from having filtration performed on a bodily fluid and identify a  
30 reservoir containing the fluid. This may include, as described above, a subject suffering from a cerebral vasospasm. Preparing the reservoir 112 may include identifying an anatomical location for a procedure to access the reservoir 112 (for example, in a spinal portion 200, as shown in FIG. 2A), sterilizing the location, or otherwise preparing the reservoir 112 for the procedure. Selecting and preparing the reservoir 112 may be  
35 performed according to the systems and methods described within this application or through other means. For example, selecting and preparing the reservoir 112 may be performed according to the various systems and methods described in U.S. Provisional Application Number 62/038,998.

5           Installing tubing 114 may include connecting various components of the system  
300. For example, retentate outlet 106 may be connected to flow regulator 118, flow  
regulator 118 to intake 304, and so on. This step may also include installing tubing 114  
to withdraw fluid from and return fluid to the reservoir 112. This step may include  
10           inserting a multi-lumen catheter into an anatomical location to place the reservoir 112 in  
fluid connection with the system 300 to enable fluid to be drawn into the intake 104 and  
returned to the reservoir 112.

          Calibrating components may include setting initial parameters for the use of the  
system 300. This step may include establishing an initial flow rate, an initial pressure,  
and other initial parameters or system settings. The initial parameters may be based on  
15           observed or predicted clinical measures, including but not limited to an estimated amount  
of fluid in the reservoir 112, the health of the subject, the predicted ratio of retentate to  
permeate, and other factors.

          Priming the system 300 may include adding a priming solution to one or more of  
the components of the system 300. Depending on the configuration of the system 300,  
20           priming may be necessary for one or more components to function effectively.  
Depending on the reservoir 112, fluid, and the subject, priming may be necessary to  
assure comfort or good health. In certain applications, the system 300 may be primed to  
enable the return of a volume of fluid while simultaneously withdrawing a volume of  
fluid. This may be especially useful for applications where the reservoir 112 has a  
25           relatively small volume of fluid (e.g., during filtration of CSF) or is otherwise sensitive  
to relative changes in volume. Depending on the type of filtration being used, the length  
of the procedure, and other factors, priming fluid may be added during the filtration  
procedure to make up for fluid lost during the procedure

          At step 404, a volume of fluid is withdrawn from the reservoir 112. In certain  
30           circumstances, the fluid may be withdrawn using a pump or device located within the  
system 100. For example, the pump may be a component of one or more of the flow  
regulators 118, 318; the filtration systems 102, 302 (such as pump 222); and/or the  
combiner 116. The pump may be used to withdraw a volume of fluid from the reservoir  
112.

35           In some embodiments, the rate at which the fluid is withdrawn from the reservoir  
112 is between approximately 0.01 mL/min and approximately 100 mL/min. In  
preferable embodiments, the fluid rate may be 0.1 mL/min to approximately 10 mL/min.  
However, the amount withdrawn may be higher or lower depending on the application.

5 The amount may vary depending on various factors including but not to the type of fluid being withdrawn, the viscosity of the fluid, the amount of fluid in the reservoir 112, and other factors. The viscosity of the fluid may vary over time, and depending on the particular subject. For example, the viscosity of CSF may be different in a subject with meningitis than a subject with typical CSF. Once the fluid is withdrawn from the  
10 reservoir 112, the fluid may pass through the tubing 114 and into the filtration system 102 via intake 104.

At step 406, the volume of fluid is filtered. This may include the steps of passing the fluid through a filter of the filtration system 102. While tangential flow filters have been described in this disclosure, they need not be the filter used, or need not be the only  
15 filter used. For example, the filtration system 102 may include various filtration component configurations including but not limited to tangential flow filtration, microfiltration, ultrafiltration, nanofiltration, dead-end filters, depth filters, and other filtration devices or mechanisms.

The filtration process may result in the separation of the fluid into a retentate  
20 flow and a permeate flow. The permeate flow may leave the filtration system 102 through a permeate outlet 108 and the retentate may leave the filtration system 102 through a retentate outlet 106. Depending on the configuration of the filters and the goals of the method 400, in some implementations, the permeate may be the fluid to be returned to the reservoir 112. In other implementations, the retentate may be returned to  
25 the reservoir 112. The retentate may be a fluid that contains contaminants or is otherwise in a condition undesirable for returning to the reservoir 112.

In certain embodiments, for example, as shown in FIG. 3, the retentate may be successively or progressively treated, such as by being filtered again through another filter process or by being filtered again through the same filter by being redirected  
30 through it. For example, in certain implementations, the retentate may be passed through a flow regulator 118 and into filtration system 302 for additional filtration. This filtration may result in the retentate being further separated into a second retentate and a second permeate. The second permeate may flow from the permeate outlet 308 to combiner 116 for return to the reservoir 112. The second retentate may be further  
35 filtered or purified. Once the fluid is sufficiently filtered, the remaining retentate or contaminants may be passed through a flow regulator 318 and into a vessel 310 for analysis, disposal, storage, or other use, or, alternatively, or in addition, the remaining retentate may be subjected to further processing, treatment, and/or filtration (any number

5 of times), where the further treated fluid is, for example, directed to reservoir 112, either directly or in combination with other fluids.

At step 408, characteristics of the fluid and/or the system may be measured. Measuring characteristics may include intermittent or continuous sampling and/or monitoring of characteristics or parameters of interest. While this step 408 is shown as  
10 occurring after the filtration of the fluid 406, the step 408 may take place at any point during the process 400 where useful data may be gathered.

In certain embodiments, measuring characteristics may include measuring the characteristics of the fluid withdrawn from the reservoir 112 before, during, or after  
15 filtration. The characteristics measured may include the presence or amount of particular contaminants, proteins, compounds, markers, and other fluid components present. As another example, the ratio of permeate volume to retentate volume, the fluid flow rate from the reservoir 112, fluid temperature, fluid opacity or translucency or transparency, an absolute retentate flow rate, and the rate of fluid flow to the reservoir 112 also may be measured. The performance characteristics of the system 300 may also be measured. For  
20 example, the efficiency of the filter 226, the status of the filter 226 (for example, via the interface 210), and other markers of system 300 performance.

In certain embodiments, the characteristics measured may include information about a subject or input by a healthcare provider. For example, the system 300 may monitor the blood pressure, heart rate, stress, and other information of the subject. In  
25 addition to quantitative characteristics, qualitative measurements may be made as well. For instance, subject discomfort and other qualities may be measured. These and other data may be measured by the sensor 224 and/or be input into the system by an input device (for example, keyboard, touch screen, subject-monitoring device, and other devices for receiving input) operably coupled to the system 300.

30 At step 410, a volume of fluid is returned to the reservoir 112. In certain embodiments, the fluid is returned to the reservoir 112 as soon as fluid filtration has been completed. In certain embodiments, the flow rate of the fluid may be controlled. For example, a volume of fluid may be buffered at the combiner 116 or in another area of the system 300 for a time before being returned to the reservoir 112. Buffering may be used  
35 to smooth the return rate of the fluid, to allow time for the fluid to reach a particular temperature, to allow time for a particular additive to mix within the fluid, and for other reasons.

5           In certain embodiments, the rate and/or pressure at which the fluid is returned to  
the reservoir 112 is controlled (for example, by the combiner 116 and/or the flow  
regulator 318). For example, the return of fluid is controlled so that the fluid is returned  
at such a rate or in such a manner as to maintain homeostasis within the reservoir 112. In  
certain embodiments, this may be accomplished by returning fluid at the same rate at  
10    which fluid is currently being withdrawn from the system. In certain embodiments, the  
fluid may be returned at substantially the same flow rate at which it was removed. The  
fluid volume removed from the system and returned to the system may not be equal. This  
may be the case when removing a significant quantity of contaminants from a reservoir.  
In certain embodiments, the difference may be made up through the addition of  
15    additional fluid.

          In certain embodiments, a particular volume of additional fluid may be returned  
to the reservoir 112. The additional fluid may be fluid that was not withdrawn from the  
reservoir 112, previously withdrawn from the reservoir 112, withdrawn from a different  
reservoir, synthetically created, or is otherwise different from the volume removed from  
20    the reservoir 112 in step 404. The return of additional fluid may be used to, for example,  
compensate for the volume of fluid that was filtered out, especially in circumstances  
where the reservoir 112 comprised only a small amount of fluid at the start 402.

          In certain embodiments, one or more therapeutic agents may be added to the fluid  
prior to its return to the reservoir 112. The fluid may be treated or mixed with a  
25    particular pharmacological agent. For example, when the fluid is CSF, the agent may be  
configured to bypass the blood-brain barrier. The agents may include, but need not be  
limited to, antibiotics, nerve growth factor, anti-inflammatory agents, pain-relief agents,  
agents designed to be delivered using intrathecal means, agents designed to affect a  
particular condition (e.g., meningitis, Alzheimer's disease, depression, chronic pain, and  
30    other conditions), and other agents.

          As a specific example, the reservoir 112 may be a CSF-containing space of a  
subject, such as the subarachnoid space or another space known or thought to contain  
CSF. The space may only have a total of approximately 125 ml of CSF, and if the level  
drops below a certain threshold (for example, approximately 85 ml), the subject may  
35    suffer undesirable side effects. If a particular large amount of the existing CSF comprises  
undesirable compounds, the volume of permeate may be small enough to cause the fluid  
levels in the reservoir 112 to drop below the threshold. Consequently, the system 300  
may return a volume of additional fluid (for example, artificial CSF or other suitable

5 fluid) to adjust for the difference between the amount of withdrawn CSF being returned and the amount needed to be returned in order to maintain the volume of the reservoir 112 above the threshold amount.

In certain embodiments, the withdrawal and return of the fluid may occur in a pulsed manner. For example, the system 300 may withdraw a particular volume and  
10 then cease withdrawing additional fluid. The withdrawn volume is processed by the filtration or other systems and be buffered (for example, at the combiner 116). Filtered amount from the buffer may be returned to the reservoir 112 at about the same rate and/or for the about same total volume as a next volume is withdrawn from the reservoir 112. This process may allow the system to maintain reservoir 112 volume levels  
15 relatively consistent and may be useful in circumstances where the processing time (for example, the time between the fluid being withdrawn from and returned to the reservoir 112) is long.

At step 412, a determination is made. The determination may be made by, for example, a healthcare professional, a processor system, or a combination thereof. For  
20 example, the healthcare professional may analyze the measure characteristics and come to a conclusion. As another example, the processing unit 208 may analyze the measured characteristics based using an algorithm or through other mechanisms. The determination may be based on the measured parameters, a timer, a schedule, or other mechanisms. The determination may be used in order to change the parameters of the  
25 system 300 to change over time and to address particular measured characteristics.

For example, a determination may be made regarding the flow rate at which the fluid is being withdrawn and/or returned to the reservoir 112. For example, it may be desirable to maintain substantially the same withdrawal and return rate of the fluid. Specifically, if more fluid is being withdrawn from the reservoir 112 than is being  
30 returned, then the volume of fluid in the reservoir 112 may be decreasing overall. This may be undesirable because for certain fluids and certain reservoirs 112, if the volume of the reservoir 112 passes a particular threshold, undesirable side effects may occur. For instance, where the fluid being withdrawn is CSF, the flow rate may be such that the volume of CSF removed from a human subject does not exceed about between  
35 approximately 5 mL and approximately 20 mL over the course of one hour. That is, the volume of fluid does not decrease more than approximately 5 mL to approximately 20 mL from its original starting volume in a one hour period of time. In certain embodiments, it may be desirable to maintain an absolute retentate flow rate within a

5 certain range of acceptable retentate flow rates. In certain embodiments, the threshold  
may be between approximately 0.10 mL/min and approximately 0.30 mL/min. In certain  
embodiments, the threshold may be approximately 0.16 mL/min. In certain  
embodiments, the threshold may be between approximately 0.2 mL/min and  
approximately 0.25 mL/min; however, other values may be desirable in certain  
10 circumstances. In certain embodiments, a pump may be running at approximately 1.0  
mL/min and the retentate flow rate is approximately 0.25 mL/min, the permeate flow rate  
is approximately 0.75 mL/min, which is about a 3:1 ratio. However, if the pump speed  
were increased to approximately 2.0 mL/min, the retentate flow rate may be held at  
approximately 0.25 mL/min, which leaves the permeate flow rate as approximately 1.75  
15 mL/min, or about a 7:1 ratio. By maintaining the retentate flow rate within the threshold,  
the system may be considering functioning as intended, despite the change in ratios.

Based on the measured characteristics, it may be determined that the best way to  
address the disparity in the withdrawal and return rates may be to decrease the flow rate  
to reduce the overall volume of fluid lost from the system. This may mean that, although  
20 there is a net loss of fluid from the reservoir 112, the loss is occurring at a slower rate.  
The rate may be sufficiently slow that, for example, that the subject's body produces  
sufficient fluid to make up for the loss.

For example, at the beginning of the filtration process 400, the fluid may contain  
large amounts of contaminants, resulting in a comparatively large amount of material  
25 being filtered out and a comparatively small amount of the fluid being returned (for  
example, permeate). As the filtration or treatment process continues, the amount of fluid  
being treated may decrease because the contaminants have already been filtered out (for  
example, retentate). In this scenario, a determination may be made to begin the process at  
a relatively low flow rate and then increase it as the volume of the fluid being filtered out  
30 decreases. In addition, the determination may include altering the flow and/or pressure  
within the filter 226 in order to achieve particular filtering results.

As another example, the measured characteristics may be a subject's expressed  
discomfort. Withdrawing CSF from a CSF-containing space of a subject may cause  
symptoms of overdrainage, such as spinal headache. Symptoms of overdrainage may be  
35 able to be avoided or otherwise addressed by not withdrawing more than a threshold  
amount of CSF. However, the particular threshold may vary from subject to subject. As  
such, a predicted threshold may be different from an actual threshold and the subject may  
experience symptoms sooner than expected. In response to the subject expressing

5 feelings of discomfort, the healthcare professional may determine that the parameters of the process may need to be changed.

In certain embodiments, at step 412, the processing unit 228 and/or a healthcare professional may determine that the process should be completed. At this point, the flow diagram moves to end step 416. In certain other embodiments, at step 412, the  
10 processing unit 228 and/or a healthcare professional may determine that the process should continue substantially unchanged. Upon that determination, the flow diagram may return to step 404. In still other embodiments, at step 412, the processing unit 228 and/or a healthcare professional may determine that the one or more parameters of the process should be changed. Upon that determination, the flow diagram may move to  
15 step 414.

At step 414, one or more parameters of the system 300 are changed in response to a determination made in step 412. The parameters to be changed may include inflow rate, outflow rate, buffer size, and other parameters. Such parameters may be changed  
20 via, for example, the processing unit 206 sending a signal to the pump 222 or other component of the system in order to modify the parameters. In certain embodiments, the parameters may be manually changed through input received at the input 208. This may include parameters entered by a healthcare professional. In certain embodiments, parameters may be updated based on the difference between the withdrawal volume and the returned volume (e.g., a waste rate).

25 In certain embodiments, the updating parameters step 414 may include changing the flow direction of the fluid. For example, a system may include a plurality of filtration systems, which the fluid may be directed to by the manipulation of a valve or other mechanisms for changing fluid flow direction. Step 414 may include changing the fluid flow from one filtration system to a different filtration. This may be in response to  
30 determining that a second filtration system (for example, filtration system 302) is more suited for filtering particular contaminants than a first filtration system (for example, filtration system 102).

In certain embodiments, the updating parameters step 414 may include modifying the positioning of the tubing at the reservoir 112. For example, one or more inflow or  
35 outflow tubes 114 may become clogged or otherwise be operating at a reduced capacity. In response, the tubing 114 may be adjusted or otherwise modified to address the reduced capacity issue. The healthcare professional may be alerted to the issue by a light, alarm or other indicia.



5           In certain embodiments, the updating parameters step 414 may include cleaning or otherwise modifying one or more components of the system 300, such as the filter 226. This may be accomplished by, for example, changing back pressure and pump speed.

10           In certain embodiments, the updating parameters step 414 may include sensing characteristics of the system to determine whether the filter 226 or other components of the system are experiencing clogging. The sensed characteristic may include reading an alert state of the filtration system or detecting an increase in filter pressure with no change to system flow rates or other parameters of the system. Responsive to determining that there may be a clog in the system 300, the flow rate through the  
15           retentate port of the filters may be increased. The increased flow rate may be the result of a user or the system opening a back pressure valve (e.g., a backpressure valve of the flow regulators 118, 318). The opening of the valve may result in a surge of fluid through one or more retentate ports of one or more filters into a waste collection area (e.g., vessels 110, 310). The surge of fluid may result in the flow returning to the reservoir 112  
20           reducing to zero or even a negative rate. Thus, the operator or system controlling the flow rate may take into account the volume of fluid lost and the possible effects on the patient as a result of this filter clearance mechanism.

          In certain embodiments, the updating parameters step 414 may include operating a fluid flow control method, such as a method 500 as shown in FIG. 5. The method 500  
25           may be used, in part, to control the flow of fluid through the system, such as the flow of retentate, permeate, waste, and/or other fluids. The fluid flow control method may include the steps of determining if the fluid flow is outside of a flow threshold 502, determining if the flow pressure is above a pressure threshold 504, stopping the pump 506, tightening a backpressure valve 508, and loosening a backpressure valve 510 (e.g., a  
30           backpressure valve of the flow regulator 118, 318 or elsewhere within a system). While fluid is flowing through the system (e.g. system 100, 300), a sensor of the system may detect a fluid flow rate (e.g., the rate at which fluid is traveling to waste, such as to vessel 110, 310) and compare it to a threshold. If the fluid flow rate is at a threshold or within a threshold range, then no substantial changes may be needed. If the fluid flow rate is  
35           above the threshold range, then the method may proceed to step 504. If the fluid flow is below the threshold range, then the method may proceed to step 510. The sensing of the flow rate may be continuous or occur periodically. In certain implementations, proceeding to the step 504, 510 need not occur immediately upon detecting a flow

5 outside of the flow threshold; instead, the method may proceed to the step 504, 510 after the flow is outside of the flow threshold for a particular number of checks (e.g., two or more checks of the waste flow rate). In certain embodiments, the threshold range for the fluid flow rate may be between approximately 0.2 mL/min and approximately 0.25 mL/min; however, other values may be used depending on particular implementations.

10 Step 504 may be reached when the fluid flow is higher than the threshold flow range. At this step, it is determined whether a pressure at or of the filter is above a pressure threshold. If the pressure is above the pressure threshold, then the method moves to step 506 and the pump is stopped. If the pressure is not above the threshold, then the method moves to step 508 where a backpressure valve is tightened and the

15 method then returns to step 502. In certain embodiments, the threshold pressure may be 1,100 mmHg; however, other thresholds may be appropriate. Step 510 may be reached if the flow rate is lower than the flow threshold. In this step, the backflow pressure valve may be loosened and the method then returns to step 502.

Returning to FIG. 4, at step 416, the process comes to an end. After the process

20 is completed, various wind-up steps may be performed, including but not limited to, applying a bandage to the subject, disassembling one or more components of the system 300, analyzing an amount of the withdrawn fluid, analyzing the retentate, and other steps.

Within this disclosure, connection references (for example, attached, coupled,

25 connected, and joined) may include intermediate members between a collection of components and relative movement between components. Such references do not necessarily infer that two components are directly connected and in fixed relation to each other. The exemplary drawings are for purposes of illustration only and the dimensions, positions, order and relative sizes reflected in the drawings attached hereto may vary.

30 The above specification provides a complete description of the structure and use of exemplary embodiments as claimed below. Although various embodiments of the invention as claimed have been described above with a certain degree of particularity, or with reference to one or more individual embodiments, those skilled in the art could make numerous alterations to the disclosed embodiments without departing from the

35 spirit or scope of this disclosure. Other embodiments are therefore contemplated. It is intended that all matter contained in the above description and shown in the accompanying drawings shall be interpreted as illustrative only of particular

- 5 embodiments and not limiting. Changes in detail or structure may be made without departing from the basic elements of the disclosure as defined in the following claims.

CLAIMS:

1. A system for filtering materials from cerebrospinal fluid (CSF) of a human or animal subject, the system comprising:

5 a filtration system configured for withdrawing a volume of fluid comprising CSF from a CSF-containing space of the subject at a first flow rate, the filtration system configured for operating according to a set of operation parameters;

a tangential flow filter configured for filtering the volume of fluid into permeate and retentate;

10 a sensor configured for measuring a characteristic of the fluid, wherein the characteristic comprises a ratio of permeate to retentate;

wherein the filtration system is configured to return the permeate to the CSF-containing space of the subject at a second flow rate; and

15 wherein the filtration system is configured to update a parameter of the set of operation parameters based on the measured characteristic responsive to determining the measured characteristic passes a predetermined threshold, wherein updating the parameter causes the first flow rate and the second flow rate to increase.

2. The system of claim 1, wherein the filtration system is configured for fluid connection with the CSF-containing space of the subject via a multi-lumen catheter configured for insertion at least partially within the space.

20 3. The system of claim 1, wherein the parameter comprises the first flow rate and the second flow rate.

4. The system of claim 3, wherein updating the parameter of the set of operation parameters further causes the first flow rate and the second flow rate to be substantially the same.

25 5. The system of claim 1, further comprising a second sensor configured for measuring a second characteristic of the fluid, wherein the second characteristic is a total volume of fluid withdrawn minus a total volume of fluid returned.

6. The system of claim 5, wherein the filtration system is configured to determine whether the second characteristic passes a second threshold, wherein the second threshold is a volume of removed CSF that is predicted to induce a spinal headache.

5 7. The system of claim 6, wherein the filtration system is configured to update a second parameter responsive to determining that the second characteristic passes the second threshold, wherein the second parameter comprises a flow rate parameter and updating the second parameter causes the first and second flow rate to decrease.

10 8. The system of claim 6, wherein the subject is a human subject and the volume of removed CSF that is predicted to induce a spinal headache is between about 35 milliliters per hour and 45 milliliters per hour.

9. The system of claim 1, wherein the rate at which the volume of fluid is configured to be withdrawn from the CSF-containing space is between approximately 0.04 milliliters per minute and approximately 30 milliliters per minute.

15 10. The system of claim 1, further comprising:  
a second sensor configured for measuring a second characteristic of the fluid, wherein the second characteristic is an absolute retentate flow rate;  
wherein the filtration system is configured to determine whether the second characteristic passes a second threshold, where the second threshold is a range of acceptable retentate flow rates; and  
20 wherein the filtration system is configured to update a second parameter of the set of operation parameters to cause the absolute retentate flow rate to return to within the range of acceptable retentate flow rates.

11. The system of claim 1, wherein the filtration system is configured to add a therapeutic agent to the permeate prior to returning the permeate.

25 12. The system of claim 1, wherein the filtration system is configured to add a volume of artificial CSF to the permeate prior to returning the permeate.

13. A system for filtering cerebrospinal fluid (CSF) of a human or animal subject, the system comprising:

a multi-lumen catheter configured to be introduced into a CSF-containing space of the subject, the catheter having a first port and a second port;

5 wherein the multi-lumen catheter is configured to withdraw a volume of fluid comprising CSF from the CSF-containing space through the first port at a withdrawal flow rate;

a tangential flow filter configured for filtering the volume of fluid into permeate and retentate by passing the volume of fluid through the tangential flow filter of the system at a pressure and a filter flow rate; and

10 wherein the multi-lumen catheter is configured to return the permeate to the CSF-containing space of the subject through the second port at a return flow rate; and

wherein the system is configured to increase the withdrawal flow rate and the return flow rate responsive to determining that a ratio of permeate to retentate has increased.

15 14. The system of claim 13, wherein the system is configured to increase at least one of the pressure and the filter flow rate responsive to determining the ratio of permeate to retentate has increased.

20 15. The system of claim 14, wherein both the pressure and the filter flow rate are configured to be increased responsive to determining the ratio of permeate to retentate has increased.

16. The system of claim 13, wherein the withdrawal flow rate and the return flow rate are configured to be substantially the same.

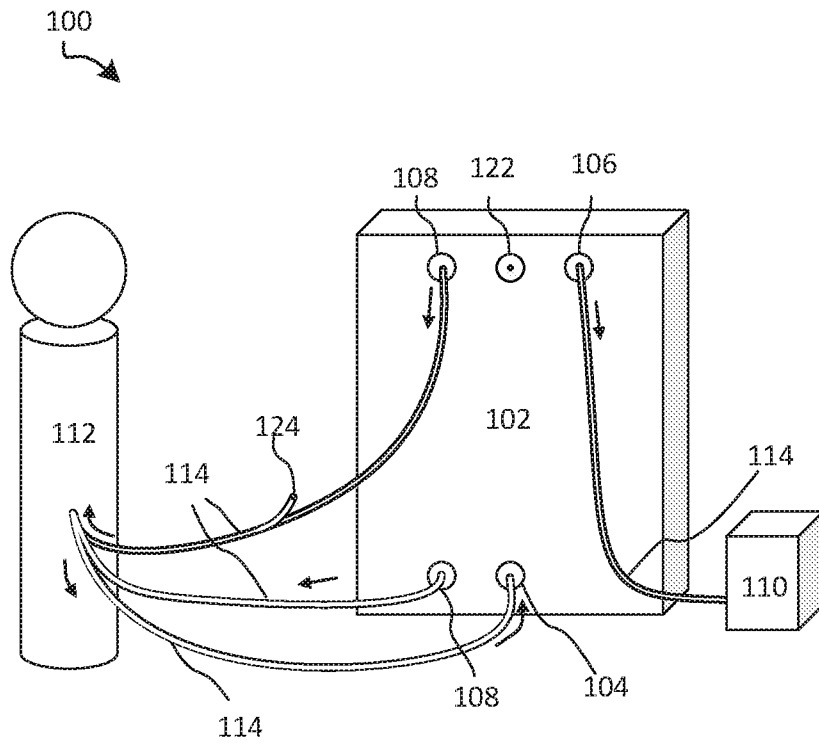


FIG. 1

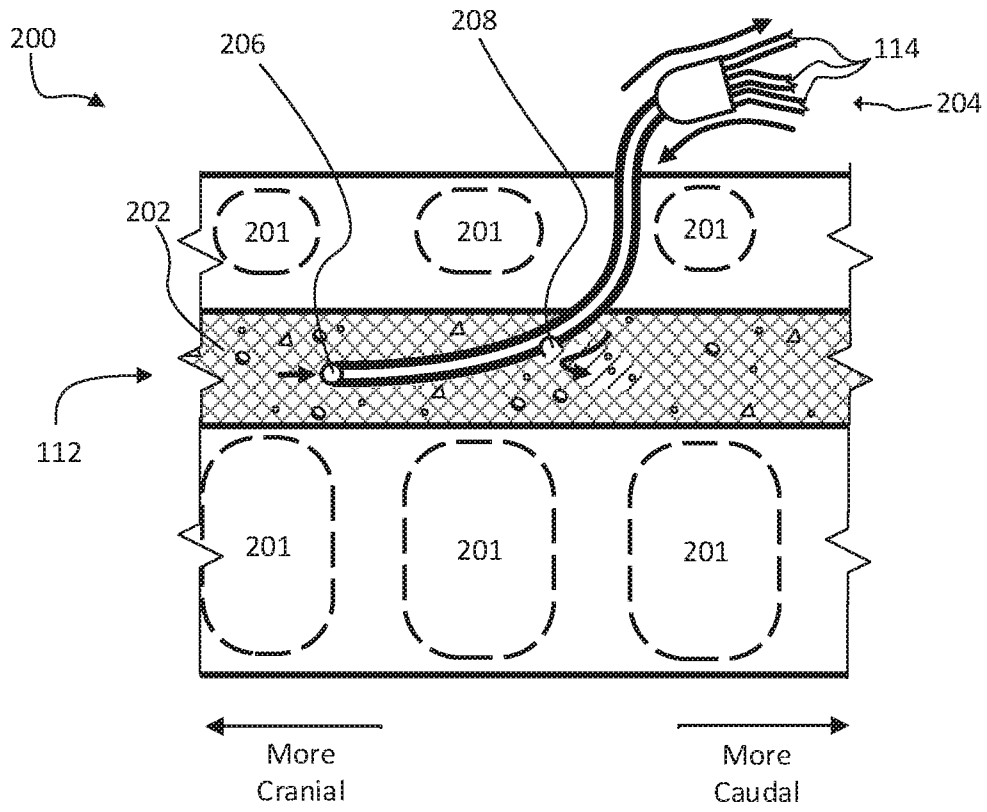


FIG.2A



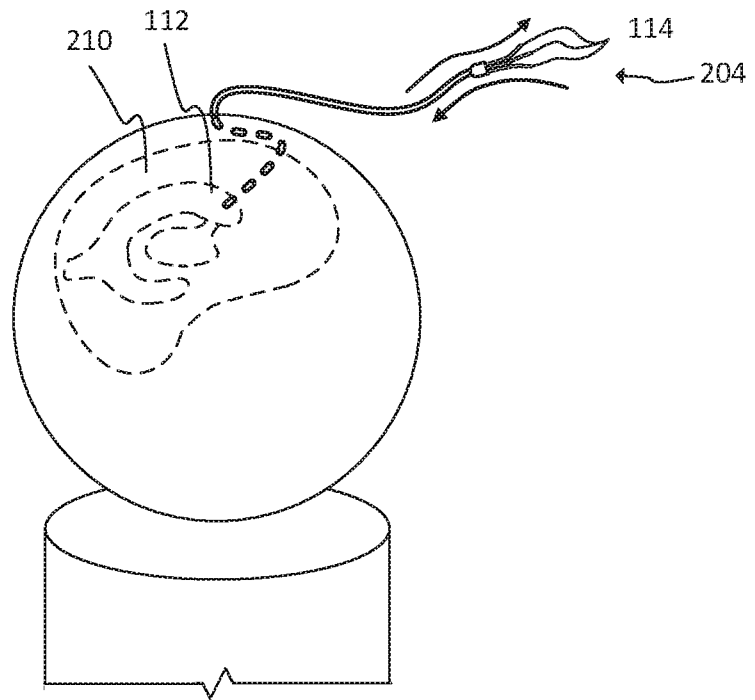


FIG.2B

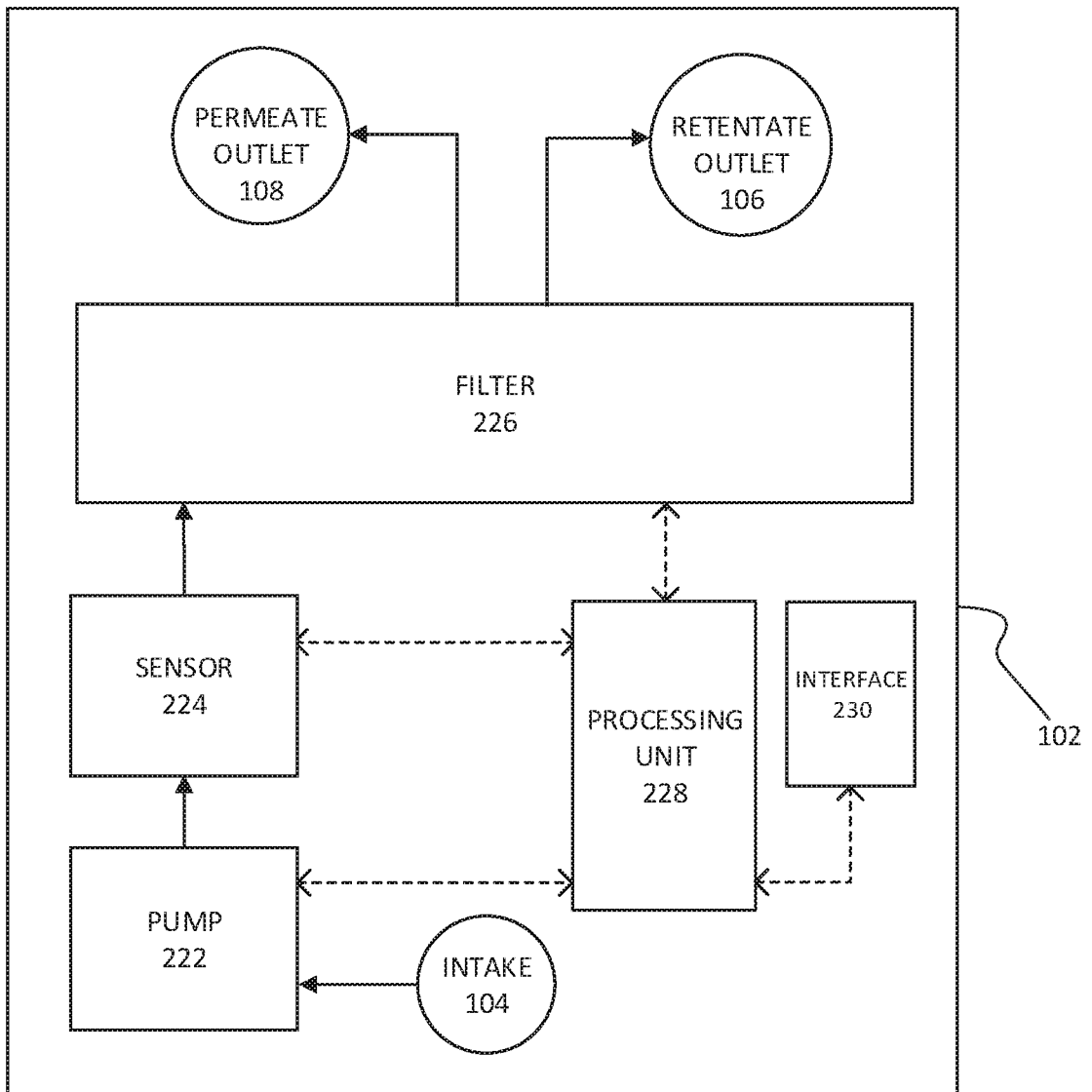


FIG. 2C

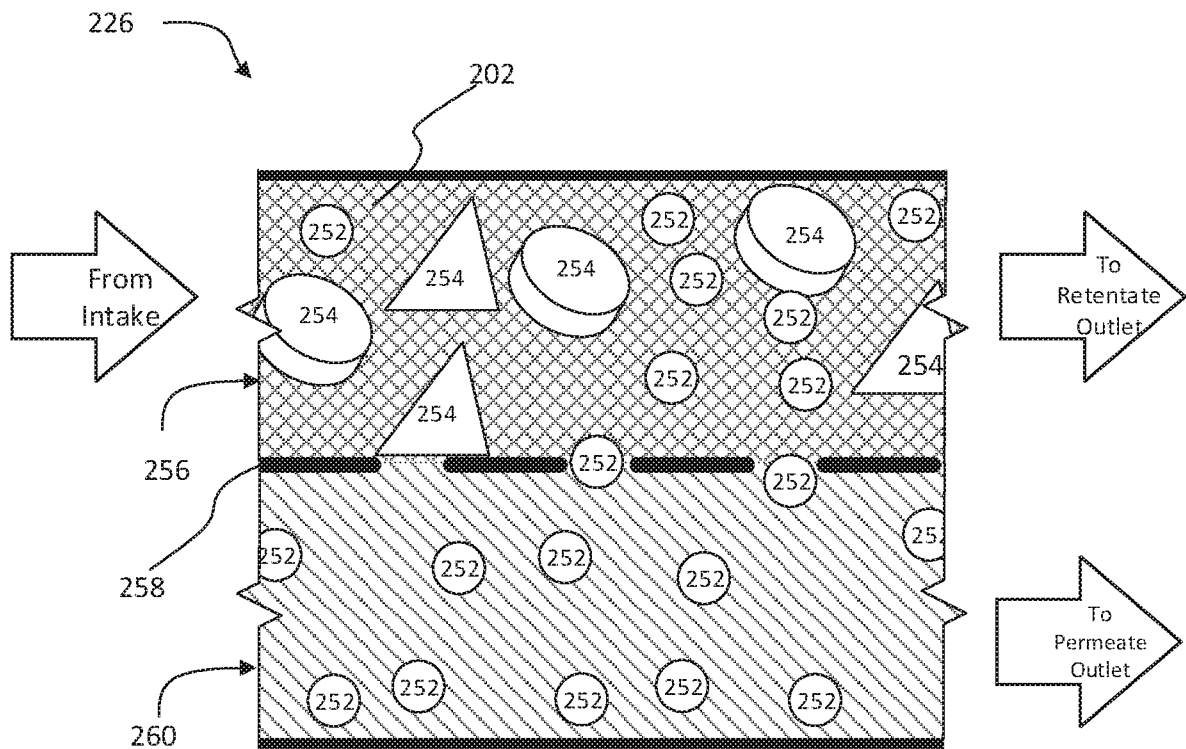


FIG. 2D

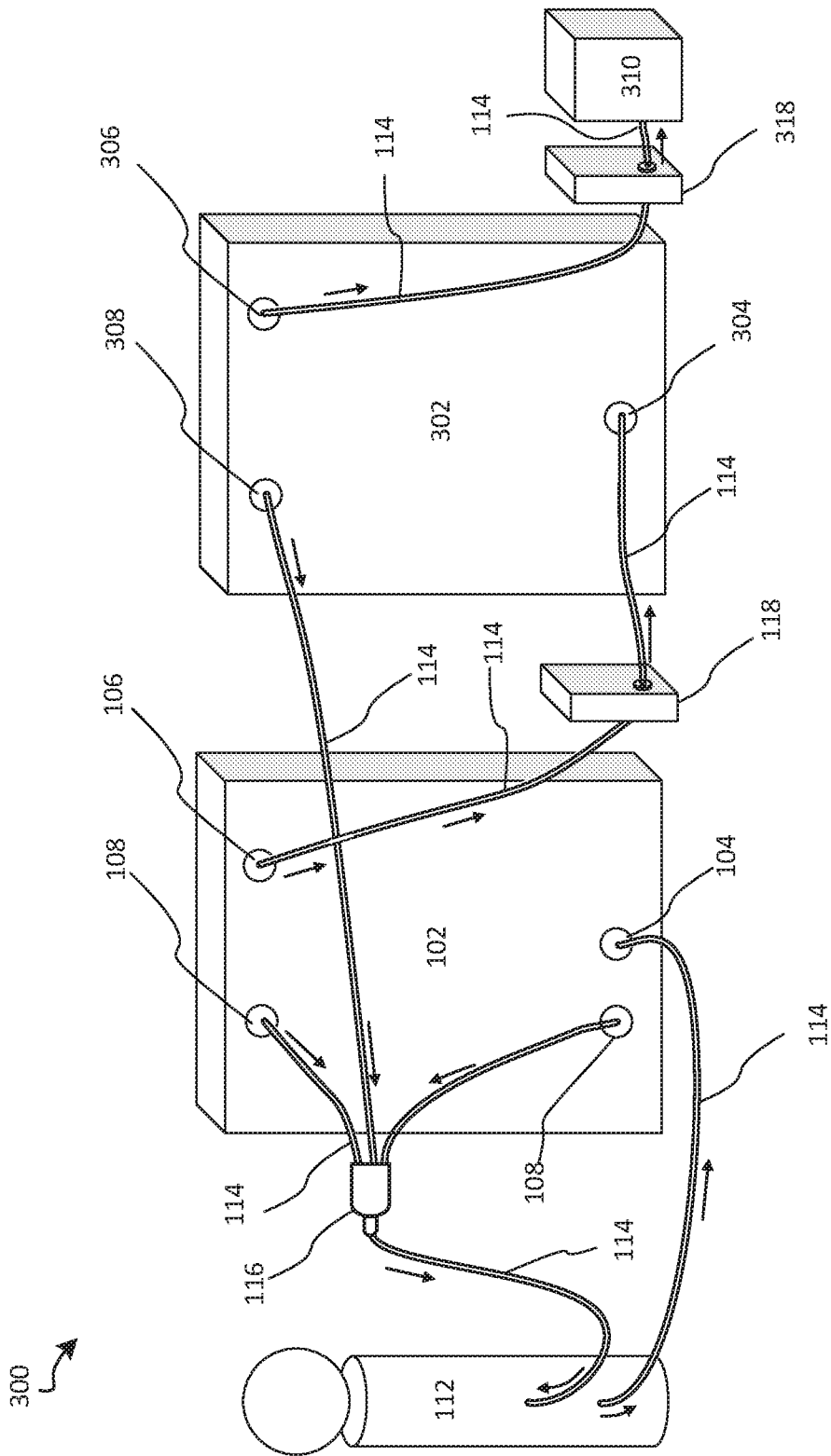


FIG. 3

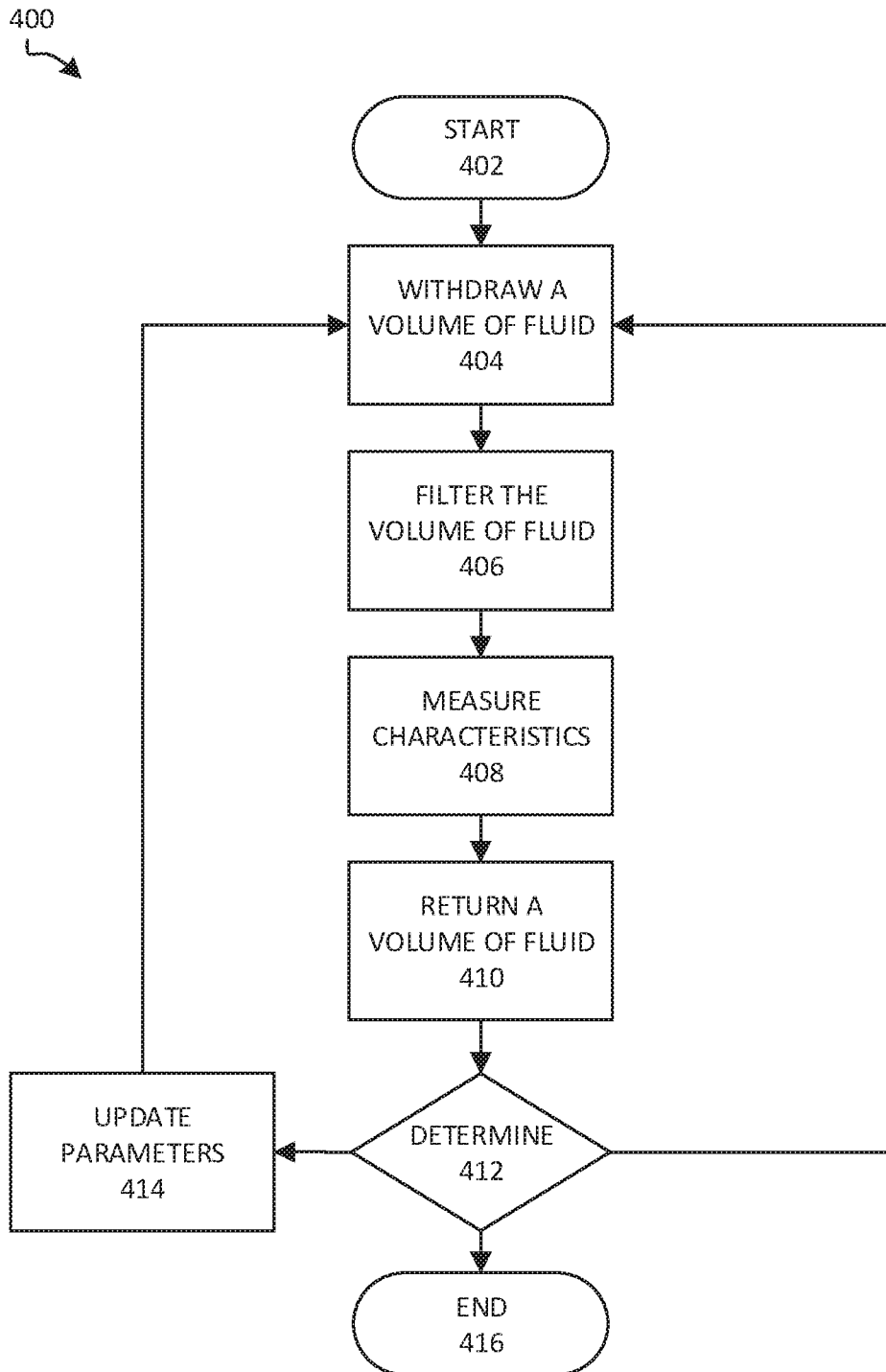


FIG. 4

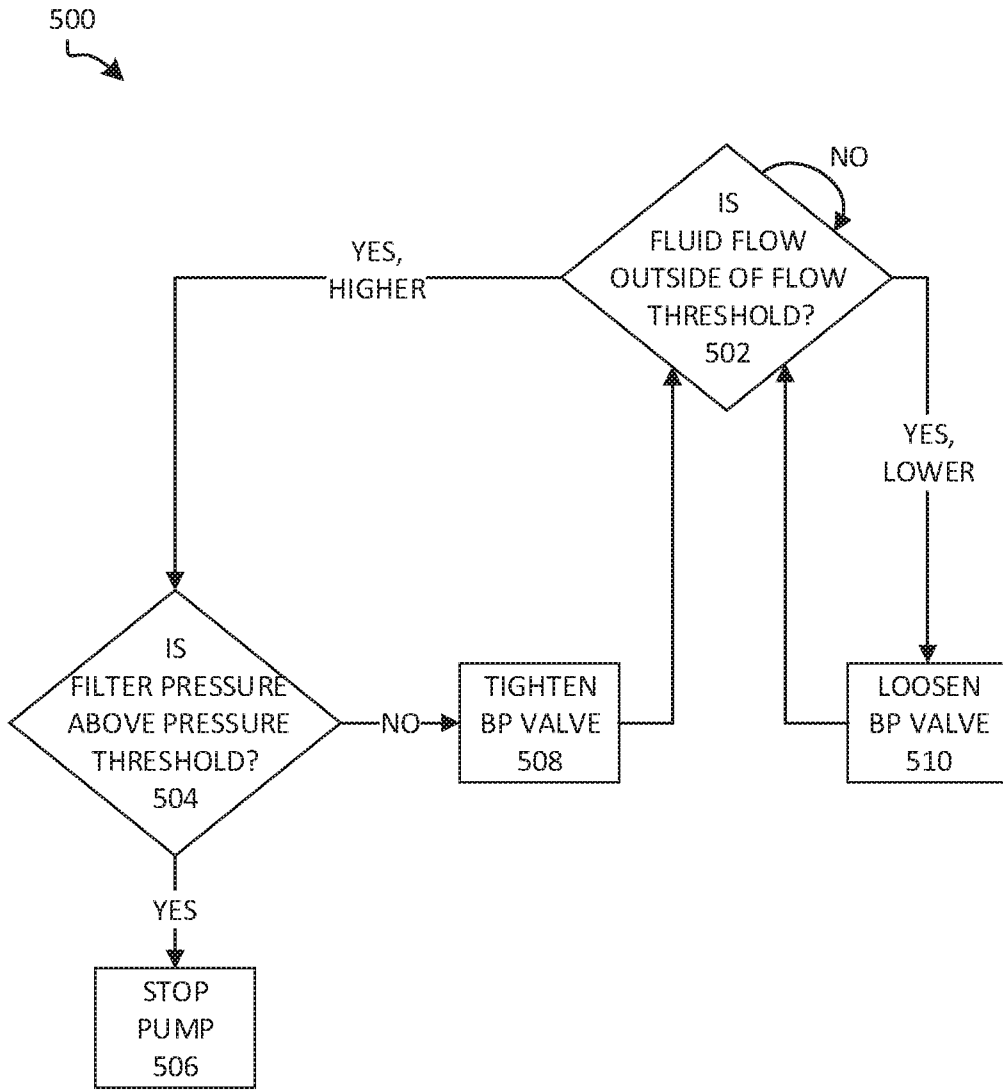


FIG. 5

100

