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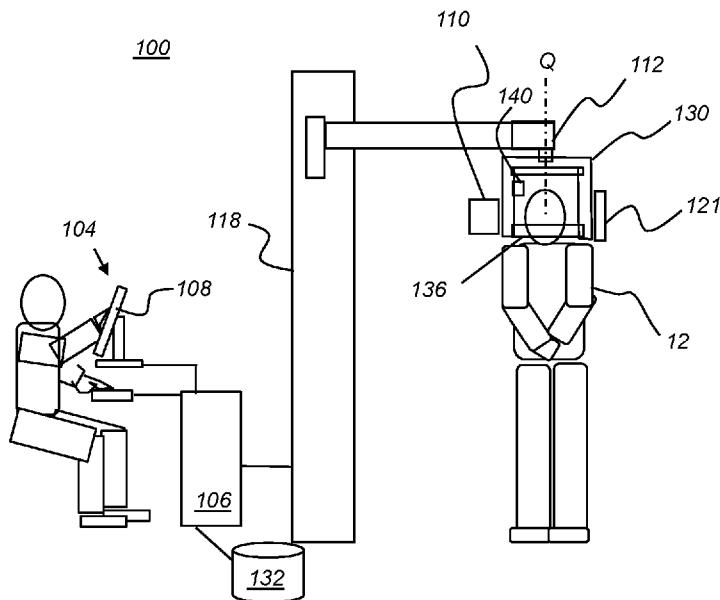


FIG. 1

(57) **Abstract:** A method for 3-D cephalometric analysis of a patient, executed at least in part on a computer processor, displays reconstructed volume image data from a computed tomographic scan of a patient's head from at least a first 2-D view and accepts an operator instruction that positions and displays at least one reference mark on the at least the first displayed 2-D view. One or more dentition elements within the mouth of the patient are segmented and cephalometric parameters for the patient computed and displayed according to data from the at least one reference mark and the one or more segmented dentition elements. Using the computed cephalometric parameters, one or more results indicative of maxillofacial asymmetry are computed and a graphical or text display energized to show the computed results indicative of asymmetry.



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## **METHOD FOR CEPHALOMETRIC ANALYSIS**

### **FIELD OF THE INVENTION**

The present invention relates generally to image processing in x-ray computed tomography and, in particular, to acquiring 3-D data for three dimensional cephalometric analysis.

### **BACKGROUND OF THE INVENTION**

Cephalometric analysis is the study of the dental and skeletal relationships for the head and is used by dentists and orthodontists as an assessment and planning tool for improved treatment of a patient. Conventional cephalometric analysis identifies bony and soft tissue landmarks in 2-D cephalometric radiographs in order to diagnose facial features and abnormalities prior to treatment, or to evaluate the progress of treatment.

For example, a dominant abnormality that can be identified in cephalometric analysis is the anteroposterior problem of malocclusion, relating to the skeletal relationship between the maxilla and mandible. Malocclusion is classified based on the relative position of the maxillary first molar. For Class I, neutroclusion, the molar relationship is normal but other teeth may have problems such as spacing, crowding, or over- or under-eruption. For Class II, distocclusion, the mesiobuccal cusp of the maxillary first molar rests between the first mandible molar and second premolar. For Class III, mesiocclusion, the mesiobuccal cusp of the maxillary first molar is posterior to the mesiobuccal grooves of the mandibular first molar.

An exemplary conventional 2-D cephalometric analysis method described by Steiner in an article entitled "Cephalometrics in Clinical Practice" (paper read at the Charles H. Tweed Foundation for Orthodontic Research, October 1956, pp. 8-29) assesses maxilla and mandible in relation to the cranial base using angular measures. In the procedure described, Steiner selects four landmarks: Nasion, Point A, Point B and Sella. The Nasion is the intersection of the frontal bone and two nasal bones of the skull. Point A is regarded as the anterior limit of the apical base of the maxilla. Point B is regarded as the anterior

limit of the apical base of the mandible. The Sella is at the mid-point of the sella turcica. The angle SNA (from Sella to Nasion, then to Point A) is used to determine if the maxilla is positioned anteriorly or posteriorly to the cranial base; a reading of about 82 degrees is regarded as normal. The angle SNB (from Sella to Nasion then to Point B) is used to determine if the mandible is positioned anteriorly or posteriorly to the cranial base; a reading of about 80 degrees is regarded as normal.

Recent studies in orthodontics indicate that there are persistent inaccuracies and inconsistencies in results provided using conventional 2-D 10 cephalometric analysis. One notable study is entitled “In vivo comparison of conventional and cone beam CT synthesized cephalograms” by Vandana Kumar et al. in *Angle Orthodontics*, September 2008, pp. 873-879.

Due to fundamental limitations in data acquisition, conventional 2-D 15 cephalometric analysis is focused primarily on aesthetics, without the concern of balance and symmetry about the human face. As stated in an article entitled “The human face as a 3D model for cephalometric analysis” by Treil et al. in *World Journal of Orthodontics*, pp. 1-6, plane geometry is inappropriate for analyzing anatomical volumes and their growth; only a 3-D diagnosis is able to 20 suitably analyze the anatomical maxillofacial complex. The normal relationship has two more significant aspects: balance and symmetry, when balance and symmetry of the model are stable, these characteristics define what is normal for each person.

U.S. Patent No. 6879712, entitled “System and method of digitally 25 modeling craniofacial features for the purposes of diagnosis and treatment predictions” to Tuncay et al., discloses a method of generating a computer model of craniofacial features. The three-dimensional facial features data are acquired using laser scanning and digital photographs; dental features are acquired by physically modeling the teeth. The models are laser scanned. Skeletal features are then obtained from radiographs. The data are combined into a single computer 30 model that can be manipulated and viewed in three dimensions. The model also has the ability for animation between the current modeled craniofacial features and theoretical craniofacial features.

U.S. Patent No. 6,250,918, entitled "Method and apparatus for simulating tooth movement for an orthodontic patient" to Sachdeva et al., discloses a method of determining a 3-D direct path of movement from a 3-D digital model of an actual orthodontic structure and a 3-D model of a desired 5 orthodontic structure. This method simulates tooth movement based on each tooth's corresponding three-dimensional direct path using laser scanned crown and markers on the tooth surface for scaling. There is no true whole tooth 3-D data using the method described.

Although significant strides have been made toward developing 10 techniques that automate entry of measurements and computation of biometric data for craniofacial features based on such measurements, there is considerable room for improvement. Even with the benefit of existing tools, the practitioner requires sufficient training in order to use the biometric data effectively. The sizable amount of measured and calculated data complicates the task of 15 developing and maintaining a treatment plan and can increase the risks of human oversight and error.

Thus it can be seen that there would be particular value in 20 development of analysis utilities that generate and report cephalometric results that can help to direct treatment planning and to track patient progress at different stages of ongoing treatment.

## **SUMMARY OF THE INVENTION**

It is an object of the present disclosure to address the need for improved ways to acquire 3-D anatomical data for cephalometric analysis. With 25 this object in mind, the present disclosure provides a method for 3-D cephalometric analysis, the method executed at least in part on a computer processor and comprising a method for 3-D cephalometric analysis of a patient, the method executed at least in part on a computer processor and comprising: displaying reconstructed volume image data from a computed tomographic scan 30 of a patient's head from at least a first 2-D view; accepting an operator instruction that positions and displays at least one reference mark on the at least the first displayed 2-D view; segmenting one or more dentition elements within the mouth

of the patient; computing and displaying a plurality of cephalometric parameters for the patient according to data from the at least one reference mark and the one or more segmented dentition elements; computing, using the computed cephalometric parameters, one or more results indicative of maxillofacial 5 asymmetry; and energizing a graphical or text display to show the computed results indicative of maxillofacial asymmetry.

A feature of the present disclosure is interaction with an operator to identify the locations of reference marks indicative of anatomical features.

10 Embodiments of the present disclosure, in a synergistic manner, integrate skills of a human operator of the system with computer capabilities for feature identification. This takes advantage of human skills of creativity, use of heuristics, flexibility, and judgment, and combines these with computer advantages, such as speed of computation, capability for exhaustive and accurate processing, and reporting and data access capabilities.

15 These and other aspects, objects, features and advantages of the present disclosure will be more clearly understood and appreciated from a review of the following detailed description of the preferred embodiments and appended claims, and by reference to the accompanying drawings.

20

## BRIEF DESCRIPTION OF THE DRAWINGS

The foregoing and other objects, features, and advantages of the invention will be apparent from the following more particular description of the embodiments of the disclosure, as illustrated in the accompanying drawings.

The elements of the drawings are not necessarily to scale relative to each other.

25 Figure 1 is a schematic diagram showing an imaging system for providing cephalometric analysis.

Figure 2 is a logic flow diagram showing processes for 3-D cephalometric analysis according to an embodiment of the present disclosure.

Figure 3 is a view of 3-D rendered CBCT head volume images.

30 Figure 4 is a view of a 3-D rendered teeth volume image after teeth segmentation.

Figure 5 is a view of a user interface that displays three orthogonal views of the CBCT head volume images and operator-entered reference marks.

Figure 6 is a view of 3-D rendered CBCT head volume images with a set of 3-D reference marks displayed.

5 Figures 7A, 7B, and 7C are perspective views that show identified anatomical features that provide a framework for cephalometric analysis.

Figure 8 is a logic flow diagram that shows steps for accepting operator instructions that generate the framework used for cephalometric analysis.

10 Figures 9A, 9B, and 9C show an operator interface for specifying the location of anatomical features using operator-entered reference marks.

Figures 10A, 10B, 10C, 10D, and 10E are graphs that show how various derived parameters are calculated using the volume image data and corresponding operator-entered reference marks.

15 Figure 11 is a 3-D graph showing a number of derived cephalometric parameters from segmented teeth data.

Figure 12 is a 2-D graph showing the derived cephalometric parameters from segmented teeth data.

Figure 13 is another 3-D graph showing the derived cephalometric parameters from segmented teeth data.

20 Figure 14 is a graph showing the derived cephalometric parameters from segmented teeth data and treatment parameter.

Figure 15 is a 3-D graph that shows how tooth exclusion is learned by the system.

25 Figure 16A is a perspective view that shows teeth of a digital phantom.

Figure 16B is a 3-D graph showing computed axes of inertia systems for upper and lower jaws.

Figure 17A is a graph showing parallelism for specific tooth structures.

30 Figure 17B is a graph showing parallelism for specific tooth structures.

Figure 18A is a perspective view that shows teeth of a digital phantom with a tooth missing.

Figure 18B is a graph showing computed axes of inertia systems for upper and lower jaws for the example of Figure 18A.

5 Figure 19A is a graph showing lack of parallelism for specific tooth structures.

Figure 19B is a graph showing lack of parallelism for specific tooth structures.

10 Figure 20A is a perspective view that shows teeth of a digital phantom with tooth exclusion.

Figure 20B is a graph showing computed axes of inertia systems for upper and lower jaws for the example of Figure 20A.

Figure 21A is an example showing tooth exclusion for a missing tooth.

15 Figure 21B is a graph showing computed axes of inertia systems for upper and lower jaws for the example of Figure 21A.

Figure 22A is an example showing tooth exclusion for a missing tooth.

20 Figure 22B is a graph showing computed axes of inertia systems for upper and lower jaws for the example of Figure 22A.

Figure 23A is an image that shows the results of excluding specific teeth.

Figure 23B is a graph showing computed axes of inertia systems for upper and lower jaws for the example of Figure 23A.

25 Figure 24 shows a number of landmarks and coordinate axes or vectors of the DOL reference system.

Figure 25 shows landmark remapping to the alternate space of the DOL reference system.

30 Figure 26 shows, from a side view, an example with transformed teeth inertia systems using this re-mapping.

Figure 27 is a schematic diagram that shows an independent network for the analysis engine according to an embodiment of the present disclosure.

5 Figure 28 is a schematic diagram that shows a dependent or coupled network for the analysis engine according to an embodiment of the present disclosure.

Figure 29 shows pseudo-code for an algorithm using the independent network arrangement of Figure 27.

10 Figure 30 shows pseudo-code for an algorithm using the dependent network arrangement of Figure 28.

Figure 31A lists example parameters as numerical values and their interpretation.

15 Figures 31B, 31C and 31D list, for a particular patient, example parameters as numerical values and their interpretation with respect to maxillofacial asymmetry, based on exemplary total maxillofacial asymmetry parameters according to exemplary embodiments of this application..

Figure 32A shows exemplary tabulated results for a particular example with bite analysis and arches angle characteristics.

20 Figure 32B shows exemplary tabulated results for a particular example for torque of upper and lower incisors.

Figure 32C shows exemplary tabulated results for another example with assessment of biretrusion or biprotrusion.

Figure 32D shows an exemplary summary listing of results for 25 cephalometric analysis of a particular patient.

Figure 32E shows a detailed listing for one of the conditions listed in Figure 35.

Figure 33 shows a system display with a recommendation message based on analysis results.

30 Figure 34 shows a system display with a graphical depiction to aid analysis results.

Figure 35 shows an exemplary report for asymmetry according to an embodiment of the present disclosure.

Figure 36 is a graph that shows relative left-right asymmetry for a patient in a front view.

Figure 37 is a graph showing relative overlap of left and right sides of a patient's face.

5 Figure 38 is a graph showing facial divergence.

## DETAILED DESCRIPTION OF THE INVENTION

In the following detailed description of embodiments of the present disclosure, reference is made to the drawings in which the same reference numerals are assigned to identical elements in successive figures. It should be noted that these figures are provided to illustrate overall functions and relationships according to embodiments of the present invention and are not provided with intent to represent actual size or scale.

15 Where they are used, the terms "first", "second", "third", and so on, do not necessarily denote any ordinal or priority relation, but may be used for more clearly distinguishing one element or time interval from another.

20 In the context of the present disclosure, the term "image" refers to multi-dimensional image data that is composed of discrete image elements. For 2-D images, the discrete image elements are picture elements, or pixels. For 3-D images, the discrete image elements are volume image elements, or voxels. The term "volume image" is considered to be synonymous with the term "3-D image".

25 In the context of the present disclosure, the term "code value" refers to the value that is associated with each 2-D image pixel or, correspondingly, each volume image data element or voxel in the reconstructed 3-D volume image. The code values for computed tomography (CT) or cone-beam computed tomography (CBCT) images are often, but not always, expressed in Hounsfield units that provide information on the attenuation coefficient of each voxel.

30 In the context of the present disclosure, the term "geometric primitive" relates to an open or closed shape such as a rectangle, circle, line, traced curve, or other traced pattern. The terms "landmark" and "anatomical

feature” are considered to be equivalent and refer to specific features of patient anatomy as displayed.

In the context of the present disclosure, the terms “viewer”, “operator”, and “user” are considered to be equivalent and refer to the viewing 5 practitioner or other person who views and manipulates an image, such as a dental image, on a display monitor. An “operator instruction” or “viewer instruction” is obtained from explicit commands entered by the viewer, such as using a computer mouse or touch screen or keyboard entry.

The term “highlighting” for a displayed feature has its conventional 10 meaning as is understood to those skilled in the information and image display arts. In general, highlighting uses some form of localized display enhancement to attract the attention of the viewer. Highlighting a portion of an image, such as an individual organ, bone, or structure, or a path from one chamber to the next, for example, can be achieved in any of a number of ways, including, but not limited 15 to, annotating, displaying a nearby or overlaying symbol, outlining or tracing, display in a different color or at a markedly different intensity or gray scale value than other image or information content, blinking or animation of a portion of a display, or display at higher sharpness or contrast.

In the context of the present disclosure, the descriptive term 20 “derived parameters” relates to values calculated from processing of acquired or entered data values. Derived parameters may be a scalar, a point, a line, a volume, a vector, a plane, a curve, an angular value, an image, a closed contour, an area, a length, a matrix, a tensor, or a mathematical expression.

The term “set”, as used herein, refers to a non-empty set, as the 25 concept of a collection of elements or members of a set is widely understood in elementary mathematics. The term “subset”, unless otherwise explicitly stated, is used herein to refer to a non-empty proper subset, that is, to a subset of the larger set, having one or more members. For a set S, a subset may comprise the complete set S. A “proper subset” of set S, however, is strictly contained in set S 30 and excludes at least one member of set S. Alternately, more formally stated, as the term is used in the present disclosure, a subset B can be considered to be a proper subset of set S if (i) subset B is non-empty and (ii) if  $B \cap S$  is also non-

empty and subset B further contains only elements that are in set S and has a cardinality that is less than that of set S.

In the context of the present disclosure, a "plan view" or "2-D view" is a 2-dimensional (2-D) representation or projection of a 3-dimensional (3-D) object from the position of a horizontal plane through the object. This term is synonymous with the term "image slice" that is conventionally used to describe displaying a 2-D planar representation from within 3-D volume image data from a particular perspective. 2-D views of the 3-D volume data are considered to be substantially orthogonal if the corresponding planes at which the views are taken are disposed at 90 (+ / - 10) degrees from each other, or at an integer multiple  $n$  of 90 degrees from each other ( $n*90$  degrees, +/- 10 degrees).

In the context of the present disclosure, the general term "dentition element" relates to teeth, prosthetic devices such as dentures and implants, and supporting structures for teeth and associated prosthetic device, including jaws.

The subject matter of the present disclosure relates to digital image processing and computer vision technologies, which is understood to mean technologies that digitally process data from a digital image to recognize and thereby assign useful meaning to human-understandable objects, attributes or conditions, and then to utilize the results obtained in further processing of the digital image.

As noted earlier in the background section, conventional 2-D cephalometric analysis has a number of significant drawbacks. It is difficult to center the patient's head in the cephalostat or other measuring device, making reproducibility unlikely. The two dimensional radiographs that are obtained produce overlapped head anatomy images rather than 3-D images. Locating landmarks on cephalograms can be difficult and results are often inconsistent (see the article entitled "Cephalometrics for the next millennium" by P. Planche and J. Treil in *The Future of Orthodontics*, ed. Carine Carels, Guy Willems, Leuven University Press, 1998, pp. 181 - 192). The job of developing and tracking a treatment plan is complex, in part, because of the significant amount of cephalometric data that is collected and calculated.

An embodiment of the present disclosure utilizes Treil's theory in terms of the selection of 3-D anatomic feature points, parameters derived from these feature points, and the way to use these derived parameters in cephalometric analysis. Reference publications authored by Treil include "The Human Face as a 5 3D Model for Cephalometric Analysis" Jacques Treil, B. Waysenson, J. Braga and J. Casteigt in *World Journal of Orthodontics*, 2005 Supplement, Vol. 6, issue 5, pp. 33-38; and "3D Tooth Modeling for Orthodontic Assessment" by J. Treil, J. Braga, J.-M. Loubes, E. Maza, J.-M. Inglese, J. Casteigt, and B. Waysenson in *Seminars in Orthodontics*, Vol. 15, No. 1, March 2009).

10 The schematic diagram of Figure 1 shows an imaging apparatus 100 for 3-D CBCT cephalometric imaging. For imaging a patient 12, a succession of multiple 2-D projection images is obtained and processed using imaging apparatus 100. A rotatable mount 130 is provided on a column 118, preferably adjustable in height to suit the size of patient 12. Mount 130 maintains an x-ray 15 source 110 and a radiation sensor 121 on opposite sides of the head of patient 12 and rotates to orbit source 110 and sensor 121 in a scan pattern about the head. Mount 130 rotates about an axis Q that corresponds to a central portion of the patient's head, so that components attached to mount 130 orbit the head. Sensor 121, a digital sensor, is coupled to mount 130, opposite x-ray source 110 that 20 emits a radiation pattern suitable for CBCT volume imaging. An optional head support 136, such as a chin rest or bite element, provides stabilization of the patient's head during image acquisition. A computer 106 has an operator interface 104 and a display 108 for accepting operator commands and for display of volume images of the orthodontia image data obtained by imaging apparatus 25 100. Computer 106 is in signal communication with sensor 121 for obtaining image data and provides signals for control of source 110 and, optionally, for control of a rotational actuator 112 for mount 130 components. Computer 106 is also in signal communication with a memory 132 for storing image data. An optional alignment apparatus 140 is provided to assist in proper alignment of the 30 patient's head for the imaging process.

Referring to the logic flow diagram of Figure 2, there is shown a sequence 200 of steps used for acquiring orthodontia data for 3-D cephalometric

analysis with a dental CBCT volume according to an embodiment of the present disclosure. The CBCT volume image data is accessed in a data acquisition step S102. A volume contains image data for one or more 2-D images (or equivalently, slices). An original reconstructed CT volume is formed using 5 standard reconstruction algorithms using multiple 2-D projections or sinograms obtained from a CT scanner. By way of example, Figure 3 shows an exemplary dental CBCT volume 202 that contains bony anatomy, soft tissues, and teeth.

Continuing with the sequence of Figure 2, in a segmentation step S104, 3-D dentition element data are collected by applying a 3-D tooth 10 segmentation algorithm to the dental CBCT volume 202. Segmentation algorithms for teeth and related dentition elements are well known in the dental imaging arts. Exemplary tooth segmentation algorithms are described, for example, in commonly assigned U.S. Patent Application Publication No. 2013/0022252 entitled “PANORAMIC IMAGE GENERATION FROM CBCT 15 DENTAL IMAGES” by Chen et al.; in U.S. Patent Application Publication No. 2013/0022255 entitled “METHOD AND SYSTEM FOR TOOTH SEGMENTATION IN DENTAL IMAGES” by Chen et al.; and in U.S. Patent Application Publication No. 2013/0022254 entitled “METHOD FOR TOOTH DISSECTION IN CBCT VOLUME” by Chen, incorporated herein by reference 20 in its entirety.

As is shown in Figure 4, tooth segmentation results are rendered with an image 302, wherein teeth are rendered as a whole but are segmented individually. Each tooth is a separate entity called a tooth volume, for example, tooth volume 304.

25 Each tooth of the segmented teeth or, more broadly, each dentition element that has been segmented has, at a minimum, a 3-D position list that contains 3-D position coordinates for each of the voxels within the segmented dentition element, and a code value list of each of the voxels within the segmented element. At this point, the 3-D position for each of the voxels is defined with 30 respect to the CBCT volume coordinate system.

In a reference mark selection step S106 in the sequence of Figure 2, the CBCT volume images display with two or more different 2-D views,

obtained with respect to different view angles. The different 2-D views can be at different angles and may be different image slices, or may be orthographic or substantially orthographic projections, or may be perspective views, for example. According to an embodiment of the present disclosure, the three views are

5 mutually orthogonal.

Figure 5 shows an exemplary format with a display interface 402 showing three orthogonal 2-D views. In display interface 402, an image 404 is one of the axial 2-D views of the CBCT volume image 202 (Figure 3), an image 406 is one of the coronal 2-D views of the CBCT volume image 202, and an image 408 is one of the sagittal 2-D views of the CBCT volume image 202. The display interface allows a viewer, such as a practitioner or technician, to interact with the computer system that executes various image processing/computer algorithms in order to accomplish a plurality of 3-D cephalometric analysis tasks. Viewer interaction can take any of a number of forms known to those skilled in the user interface arts, such as using a pointer such as a computer mouse joystick or touchpad, or using a touch screen for selecting an action or specifying a coordinate of the image, for interaction described in more detail subsequently.

One of the 3-D cephalometric analysis tasks is to perform automatic identification in 3-D reference mark selection step S106 of Figure 2. 20 The 3-D reference marks, equivalent to a type of 3-D landmark or feature point identified by the viewer on the displayed image, are shown in the different mutually orthogonal 2-D views of display interface 402 in Figure 5. Exemplary 3-D anatomic reference marks shown in Figure 5 are lower nasal palatine foramen at reference mark 414. As shown in the view of Figure 6, other anatomic 25 reference marks that can be indicated by the viewer on a displayed image 502 include infraorbital foramina at reference marks 508 and 510, and malleus at reference marks 504 and 506.

In step S106 of Figure 2, the viewer uses a pointing device (such as a mouse or touch screen, for example) to place a reference mark as a type of 30 geometric primitive at an appropriate position in any one of the three views. According to an embodiment of the present disclosure that is shown in figures herein, the reference mark displays as a circle. Using the display interface screen

of Figure 5, for example, the viewer places a small circle in the view shown as image 404 at location 414 as the reference mark for a reference point. Reference mark 414 displays as a small circle in image 404 as well as at the proper position in corresponding views in images 406 and 408. It is instructive to note that the 5 viewer need only indicate the location of the reference mark 414 in one of the displayed views 404, 406 or 408; the system responds by showing the same reference mark 414 in other views of the patient anatomy. Thus, the viewer can identify the reference mark 414 in the view in which it is most readily visible.

After entering the reference mark 414, the user can use operator 10 interface tools such as the keyboard or displayed icons in order to adjust the position of the reference mark 414 on any of the displayed views. The viewer also has the option to remove the entered reference mark and enter a new one.

The display interface 402 (Figure 5) provides zoom in/out utilities 15 for re-sizing any or all of the displayed views. The viewer can thus manipulate the different images efficiently for improved reference mark positioning.

The collection of reference marks made with reference to and appearing on views of the 3-D image content, provides a set of cephalometric parameters that can be used for a more precise characterization of the patient's head shape and structure. Cephalometric parameters include coordinate 20 information that is provided directly by the reference mark entry for particular features of the patient's head. Cephalometric parameters also include information on various measurable characteristics of the anatomy of a patient's head that are not directly entered as coordinate or geometric structures but are derived from coordinate information, termed "derived cephalometric parameters". Derived 25 cephalometric parameters can provide information on relative size or volume, symmetry, orientation, shape, movement paths and possible range of movement, axes of inertia, center of mass, and other data. In the context of the present disclosure, the term "cephalometric parameters" applies to those that are either directly identified, such as by the reference marks, or those derived cephalometric 30 parameters that are computed according to the reference marks. For example, as particular reference points are identified by their corresponding reference marks, framework connecting lines 522 are constructed to join the reference points for a

suitable characterization of overall features, as is more clearly shown in Figure 6. Framework connecting lines 522 can be considered as vectors in 3-D space; their dimensional and spatial characteristics provide additional volume image data that can be used in computation for orthodontia and other purposes.

5            Each reference mark 414, 504, 506, 508, 510 is the terminal point for one or more framework connecting lines 522, generated automatically within the volume data by computer 106 of image processing apparatus 100 and forming a framework that facilitates subsequent analysis and measurement processing. Figures 7A, 7B, and 7C show, for displayed 3-D images 502a, 502b, and 502c  
10          from different perspective views, how a framework 520 of selected reference points, with the reference points at the vertices, helps to define dimensional aspects of the overall head structure. According to an embodiment of the present disclosure, an operator instruction allows the operator to toggle between 2-D views similar to those shown in Figure 5 and the volume representation shown in  
15          Figure 6, with partial transparency for voxels of the patient's head. This enables the operator to examine reference mark placement and connecting line placement from a number of angles; adjustment of reference mark position can be made on any of the displayed views. In addition, according to an embodiment of the present disclosure, the operator can type in more precise coordinates for a specific  
20          reference mark.

          The logic flow diagram of Figure 8 shows steps in a sequence for accepting and processing operator instructions for reference mark entry and identification and for providing computed parameters according to the image data and reference marks. A display step S200 displays one or more 2-D views, from  
25          different angles, such as from mutually orthogonal angles, for example, of reconstructed 3-D image data from a computed tomographic scan of a patient's head. In an optional listing step S210, the system provides a text listing such as a tabular list, a series of prompts, or a succession of labeled fields for numeric entry that requires entry of positional data for a number of landmarks or anatomical  
30          features in the reconstructed 3-D image. This listing may be explicitly provided for the operator in the form of user interface prompts or menu selection, as described subsequently. Alternately, the listing may be implicitly defined, so that

the operator need not follow a specific sequence for entering positional information. Reference marks that give the x, y, z positional data for different anatomical features are entered in a recording step S220. Anatomical features can lie within or outside of the mouth of the patient. Embodiments of the present disclosure can use a combination of anatomical features identified on the display, as entered in step S220, and segmentation data automatically generated for teeth and other dentition elements, as noted previously with reference to Figure 2.

In recording step S220 of Figure 8, the system accepts operator instructions that position a reference mark corresponding to each landmark feature of the anatomy. The reference mark is entered by the operator on either the first or the second 2-D view, or on any of the other views if more than two views are presented and, following entry, displays on each of the displayed views. An identification step S230 identifies the anatomical feature or landmark that corresponds to the entered reference mark and, optionally, verifies the accuracy of the operator entry. Proportional values are calculated to determine the likelihood that a given operator entry accurately identifies the position of a reference mark for a particular anatomical feature. For example, the infraorbital foramen is typically within a certain distance range from the palatine foramen; the system checks the entered distance and notifies the operator if the corresponding reference mark does not appear to be properly positioned.

Continuing with the sequence of Figure 8, in a construction step S240, framework connecting lines are generated to connect reference marks for frame generation. A computation and display step S250 is then executed, computing one or more cephalometric parameters according to the positioned reference marks. The computed parameters are then displayed to the operator.

Figures 9A, 9B, and 9C show an operator interface appearing on display 108. The operator interface provides, on display 108, an interactive utility for accepting operator instructions and for displaying computation results for cephalometric parameters of a particular patient. Display 108 can be a touch screen display for entry of operator-specified reference marks and other instructions, for example. Display 108 simultaneously displays at least one 2-D view of the volume image data or two or more 2-D views of the volume image

data from different angles or perspectives. By way of example, Figure 9A shows a frontal or coronal view 150 paired with a side or sagittal view 152. More than two views can be shown simultaneously and different 2-D views can be shown, with each of the displayed views independently positioned according to an

5 embodiment of the present disclosure. Views can be mutually orthogonal or may simply be from different angles. As part of the interface of display 108, an optional control 166 enables the viewer to adjust the perspective angle from which one or more of the 2-D views are obtained, either by toggling between alternate fixed views or by changing the relative perspective angle in increments along any

10 of the 3-D axes (x, y, z). A corresponding control 166 can be provided with each 2-D view, as shown in Figure 9-C. Using the operator interface shown for display 108, each reference mark 414 is entered by the operator using a pointer of some type, which may be a mouse or other electronic pointer or may be a touchscreen entry as shown in Figure 9A. As part of the operator interface, an optional listing

15 156 is provided to either guide the operator to enter a specific reference mark according to a prompt, or to identify the operator entry, such as by selection from a drop-down menu 168 as shown in the example of Figure 9B. Thus, the operator can enter a value in listing 156 or may enter a value in field 158, then select the name associated with the entered value from drop-down menu 168. Figures 9A-

20 9C show a framework 154 constructed between reference points. As Figure 9A shows, each entered reference mark 414 may be shown in both views 150 and 152. A selected reference mark 414 is highlighted on display 108, such as appearing in bold or in another color. A particular reference mark is selected in order to obtain or enter information about the reference mark or to perform some

25 action, such as to shift its position, for example.

In the embodiment shown in Figure 9B, the reference mark 414 just entered or selected by the operator is identified by selection from a listing 156. For the example shown, the operator selects the indicated reference mark 414, then makes a menu selection such as “infraorbital foramen” from menu 168.

30 An optional field 158 identifies the highlighted reference mark 414. Calculations based on a model or based on standard known anatomical relationships can be used to identify reference mark 414, for example.

Figure 9C shows an example in which the operator enters a reference mark 414 instruction that is detected by the system as incorrect or unlikely. An error prompt or error message 160 displays, indicating that the operator entry appears to be in error. The system computes a probable location for a particular landmark or 5 anatomical feature based on a model or based on learned data, for example. When the operator entry appears to be inaccurate, message 160 displays, along with an optional alternate location 416. An override instruction 162 is displayed, along with a repositioning instruction 164 for repositioning the reference mark according to the calculated information from the system. Repositioning can be 10 done by accepting another operator entry from the display screen or keyboard or by accepting the system-computed reference mark location, at alternate location 416 in the example of Figure 9C.

According to an alternate embodiment of the present disclosure, the operator does not need to label reference marks as they are entered. Instead the 15 display prompts the operator to indicate a specific landmark or anatomical feature on any of the displayed 2-D views and automatically labels the indicated feature. In this guided sequence, the operator responds to each system prompt by indicating the position of the corresponding reference mark for the specified landmark.

20 According to another alternate embodiment of the present disclosure, the system determines which landmark or anatomical feature has been identified as the operator indicates a reference mark; the operator does not need to label reference marks as they are entered. The system computes the most likely reference mark using known information about anatomical features that have 25 already been identified and, alternately, by computation using the dimensions of the reconstructed 3-D image itself.

Using the operator interface shown in the examples of Figures 9A-9C, embodiments of the present disclosure provide a practical 3-D cephalometric analysis system that synergistically integrates the skills of the human operator of 30 the system with the power of the computer in the process of 3-D cephalometric analysis. This takes advantage of human skills of creativity, use of heuristics, flexibility, and judgment, and combines these with computer advantages, such as

speed of computation, capability for accurate and repeatable processing, reporting and data access and storage capabilities, and display flexibility.

Referring back to the sequence of Figure 2, derived cephalometric parameters are computed in a computation step S108 once a sufficient set of landmarks is entered. Figures 10A through 10E show a processing sequence for computing and analyzing cephalometric data and shows how a number of cephalometric parameters are obtained from combined volume image data and anatomical features information according to operator entered instructions and according to segmentation of the dentition elements. According to an embodiment of the present disclosure, portions of the features shown in Figures 10A through 10E are displayed on display 108 (Figure 1).

An exemplary derived cephalometric parameter shown in Figure 10A is a 3-D plane 602 (termed a t-reference plane in cephalometric analysis) that is computed by using a subset of the set of first geometric primitives with reference marks 504, 506, 508 and 510 as previously described with reference to Figure 6. A further derived cephalometric parameter is 3-D coordinate reference system 612 termed a t-reference system and described by Treil in publications noted previously. The z axis of the t-reference system 612 is chosen as perpendicular to the 3-D t-reference plane 602. The y axis of the t-reference system 612 is aligned with framework connecting line 522 between reference marks 508 and 504. The x axis of the t-reference system 612 is in plane 602 and is orthogonal to both z and x axes of the t-reference system. The directions of t-reference system axes are indicated in Figure 10A and in subsequent Figures 10B, 10C, 10D, and 10E. The origin of the t-reference system is at the middle of framework connecting line 522 that connects reference marks 504 and 506.

With the establishment of t-reference system 612, 3-D reference marks from step S106 and 3-D teeth data (3-D position list of a tooth) from step S104 are transformed from the CBCT volume coordinate system to t-reference system 612. With this transformation, subsequent computations of derived cephalometric parameters and analyses can now be performed with respect to t-reference system 612.

Referring to Figure 10B, a 3-D upper jaw plane 704 and a 3-D lower jaw plane 702 can be derived from cephalometric parameters from the teeth data in t-reference system 612. The derived upper jaw plane 704 is computed according to teeth data segmented from the upper jaw (maxilla). Using methods 5 familiar to those skilled in cephalometric measurement and analysis, derived lower jaw plane 702 is similarly computed according to the teeth data segmented from the lower jaw (mandibular).

For an exemplary computation of a 3-D plane from the teeth data, an inertia tensor is formed by using the 3-D position vectors and code values of 10 voxels of all teeth in a jaw (as described in the cited publications by Treil); eigenvectors are then computed from the inertia tensor. These eigenvectors mathematically describe the orientation of the jaw in the t-reference system 612. A 3-D plane can be formed using two of the eigenvectors, or using one of the eigenvectors as the plane normal.

15 Referring to Figure 10C, further derived parameters are shown. For each jaw, jaw curves are computed as derived parameters. An upper jaw curve 810 is computed for the upper jaw; a lower jaw curve 812 is derived for the lower jaw. The jaw curve is constructed to intersect with the mass center of each tooth in the respective jaw and to lie in the corresponding jaw plane. The mass 20 center of the tooth can be calculated, in turn, using the 3-D position list and the code value list for the segmented teeth.

The mass of a tooth is also a derived cephalometric parameter computed from the code value list of a tooth. In Figure 10C, an exemplary tooth mass is displayed as a circle 814 or other type of shape for an upper jaw tooth. 25 According to an embodiment of the present disclosure, one or more of the relative dimensions of the shape, such as the circle radius, for example, indicates relative mass value, the mass value of the particular tooth in relation to the mass of other teeth in the jaw. For example, the first molar of the upper jaw has a mass value larger than the neighboring teeth mass values.

30 According to an embodiment of the present disclosure, for each tooth, an eigenvector system is also computed. An inertia tensor is initially formed by using the 3-D position vectors and code values of voxels of a tooth, as

described in the cited publications by Treil. Eigenvectors are then computed as derived cephalometric parameters from the inertia tensor. These eigenvectors mathematically describe the orientation of a tooth in the t-reference system.

As shown in Figure 10D, another derived parameter, an occlusal 5 plane, 3-D plane 908, is computed from the two jaw planes 702 and 704. Occlusal plane, 3-D plane 908, lies between the two jaw planes 702 and 704. The normal of plane 908 is the average of the normal of plane 702 and normal of plane 704.

For an individual tooth, in general, the eigenvector corresponding 10 to the largest computed eigenvalue is another derived cephalometric parameter that indicates the medial axis of the tooth. Figure 10E shows two types of exemplary medial axes for teeth: medial axes 1006 for upper incisors and medial axes 1004 for lower incisors.

The calculated length of the medial axis of a tooth is a useful 15 cephalometric parameter in cephalometric analysis and treatment planning along with other derived parameters. It should be noted that, instead of using the eigenvalue to set the length of the axis as proposed in the cited publication by Triel, embodiments of the present disclosure compute the actual medial axis length as a derived parameter using a different approach. A first intersection point of the medial axis with the bottom slice of the tooth volume is initially located. 20 Then, a second intersection point of the medial axis with the top slice of the tooth volume is identified. An embodiment of the present disclosure then computes the length between the two intersection points.

Figure 11 shows a graph 1102 that provides a closeup view that isolates the occlusal plane 908 in relation to upper jaw plane 704 and lower jaw 25 plane 702 and shows the relative positions and curvature of jaw curves 810 and 812.

Figure 12 shows a graph 1202 that shows the positional and angular relationships between the upper teeth medial axes 1006 and the lower teeth medial axes 1004.

30 As noted in the preceding descriptions and shown in the corresponding figures, there are a number of cephalometric parameters that can be derived from the combined volume image data, including dentition element

segmentation, and operator-entered reference marks. These are computed in a computer-aided cephalometric analysis step S110 (Figure 2).

One exemplary 3-D cephalometric analysis procedure in step S110 that can be particularly valuable relates to the relative parallelism of the maxilla 5 (upper jaw) and mandibular (lower jaw) planes 702 and 704. Both upper and lower jaw planes 702 and 704, respectively, are derived parameters, as noted previously. The assessment can be done using the following sequence:

- Project the x axis of the maxilla inertia system (that is, the eigenvectors) to the x-z plane of the t-reference system and compute an angle MX1\_RF between the z axis of the t-reference system and the projection;
- Project the x axis of the mandibular inertia system (that is, the eigenvectors) to the x-z plane of the t-reference system and compute an angle MD1\_RF between the z axis of the t-reference system and the projection;
- MX1\_MD1\_RF = MX1\_RF - MD1\_RF gives a parallelism assessment of upper and lower jaws in the x-z plane of the t-reference system;
- Project the y axis of the maxilla inertia system (that is, the eigenvectors) to the y-z plane of the t-reference system and compute the angle MX2\_RS between the y axis of the t-reference system and the projection;
- Project the y axis of the mandibular inertia system (that is, the eigenvectors) to the y-z plane of the t-reference system and compute an angle MD2\_RS between the y axis of the t-reference system and the projection;
- MX2\_MD2\_RS = MX2\_RS - MD2\_RS gives a parallelism assessment of upper and lower jaws in the y-z plane of the t-reference system.

Another exemplary 3-D cephalometric analysis procedure that is executed in step S110 is assessing the angular property between the maxilla (upper jaw) incisor and mandible (lower jaw) incisor using medial axes 1006 and 1004 (Figures 10E, 12). The assessment can be done using the following 30 sequence:

- Project the upper incisor medial axis 1006 to the x-z plane of the t-reference system and compute an angle MX1\_AF between the z axis of the t-reference system and the projection;
- Project the lower incisor medial axis 1004 to the x-z plane of the t-reference system and compute an angle MD1\_AF between the z axis of the t-reference system and the projection;
- MX1\_MD1\_AF = MX1\_AF - MD1\_AF gives the angular property assessment of the upper and lower incisors in the x-z plane of the t-reference system;
- 10 • Project the upper incisor medial axis 1006 to the y-z plane of the t-reference system and compute an angle MX2\_AS between the y axis of the t-reference system and the projection;
- Project the lower incisor medial axis 1004 to the y-z plane of the t-reference system and compute an angle MD2\_AS between the y axis of the t-reference system and the projection;
- 15 • MX2\_MD2\_AS = MX2\_AS - MD2\_AS gives the angular property assessment of upper and lower incisors in the y-z plane of the t-reference system.

Figure 13 shows a graph 1300 that shows a local x-y-z coordinate system 1302 for an upper incisor, and a local x-y-z coordinate system 1304 for a lower incisor. The local axes of the x-y-z coordinate system align with the eigenvectors associated with that particular tooth. The x axis is not shown but satisfies the right-hand system rule.

In Figure 13, the origin of system 1302 can be selected at any place along axis 1006. An exemplary origin for system 1302 is the mass center of the tooth that is associated with axis 1006. Similarly, the origin of system 1304 can be selected at any place along axis 1004. An exemplary origin for system 1304 is the mass center of the tooth that is associated with axis 1004.

Based on the analysis performed in Step S110 (Figure 2), an adjustment or treatment plan is arranged in a planning step S112. An exemplary treatment plan is to rotate the upper incisor counter clockwise at a 3-D point, such as at its local coordinate system origin, and about an arbitrary 3-D axis, such as

about the x axis of the local x-y-z system. The graph of Figure 14 shows rotation to an axis position 1408.

In a treatment step S114 of Figure 2, treatment is performed based on the planning, for example, based on upper incisor rotation. The treatment 5 planning can be tested and verified visually in a visualization step S116 before the actual treatment takes place.

Referring back to Figure 2, there is shown a line 120 from Step S114 to Step S102. This indicates that there is a feedback loop in the sequence 200 workflow. After the patient undergoes treatment, an immediate evaluation or, 10 alternately, a scheduled evaluation of the treatment can be performed by entering relevant data as input to the system. Exemplary relevant data for this purpose can include results from optical, radiographic, MRI, or ultrasound imaging and/or any meaningful related measurements or results.

An optional tooth exclusion step S124 is also shown in sequence 15 200 of Figure 2. For example, if the patient has had one or more teeth removed, then the teeth that complement the removed teeth can be excluded. For this step, the operator specifies one or more teeth, if any, to be excluded from the rest of the processing steps based on Treil's theory of jaw planes parallelism. The graph of Figure 15 shows how tooth exclusion can be learned by the system, using a virtual 20 or digital phantom 912. Digital phantom 912 is a virtual model used for computation and display that is constructed using a set of landmarks and a set of upper teeth of a digital model of an upper jaw and a set of lower teeth of a digital model of a lower jaw. Digital phantom 912 is a 3-D or volume image data model that is representative of image data that is obtained from patient anatomy and is 25 generated using the landmark and other anatomical information provided and can be stored for reference or may be generated for use as needed. The use of various types of digital phantom is well known to those skilled in the digital radiography arts. The landmarks such as reference marks 504, 506, 508 and 510 of the digital phantom 912 correspond to the actual reference marks identified from the CBCT 30 volume 202 (Figure 3). These landmarks are used to compute the t-reference system 612 (Figures 10A-10E).

The operator can exclude one or more teeth by selecting the teeth from a display or by entering information that identifies the excluded teeth on the display.

In the Figure 15 representation, the upper and lower teeth, such as 5 digital teeth 2202 and 2204 of digital phantom 912 are digitally generated. The exemplary shape of a digital tooth is a cylinder, as shown. The exemplary voxel value for a digital tooth in this example is 255. It can be appreciated that other shapes and values can be used for phantom 912 representation and processing.

Figure 16A shows digital teeth 2202 and 2204 of digital phantom 10 912. The corresponding digital teeth in the upper digital jaw and lower digital jaw are generated in a same way, with the same size and same code value.

To assess parallelism of the upper and lower digital jaws, an inertia tensor for each digital jaw is formed by using the 3-D position vectors and code values of voxels of all digital teeth in a digital jaw (see the Treil publications, 15 cited previously). Eigenvectors are then computed from the inertia tensor. These eigenvectors, as an inertial system, mathematically describe the orientation of the jaw in the t-reference system 612 (Figure 10A). As noted earlier, the eigenvectors, computed from the inertial tensor data, are one type of derived cephalometric parameter.

20 As shown in Figure 16B, the computed axes of an upper digital jaw inertia system 2206 and a lower digital jaw inertia system 2208 are in parallel for the generated digital phantom 912 as expected, since the upper and lower jaw teeth are created in the same way. Figure 17A shows this parallelism in the sagittal view along a line 2210 for the upper jaw and along a line 2212 for the 25 lower jaw; Figure 17B shows parallelism in the frontal (coronal) view at a line 2214 for the upper jaw and at a line 2216 for the lower jaw.

Referring to Figures 18A and 18B, there is shown a case in which 30 digital tooth 2204 is missing. The computed axes of upper digital jaw inertia system 2206 and lower digital jaw inertia system 2208 are no longer in parallel. In corresponding Figures 19A and 19B, this misalignment can also be examined in a sagittal view along a line 2210 for the upper jaw and a line 2212 for the lower jaw; in the frontal view along a line 2214 for the upper jaw and a line 2216 for the

lower jaw. According to an embodiment of the present disclosure, this type of misalignment of upper and lower jaw planes (inertia system) due to one or more missing teeth can be corrected by excluding companion teeth of each missing tooth as illustrated in Figures 20A and 20B. The companion teeth for tooth 2204 5 are teeth 2304, 2302 and 2202. Tooth 2304 is the corresponding tooth in the upper jaw for tooth 2204. Teeth 2202 and 2302 are the corresponding teeth at the other side for the teeth 2304 and 2204. After excluding the companion teeth for the missing tooth 2204, the computed axes of inertia system 2206 for the upper jaw and inertia system 2208 for the lower jaw are back in parallel.

10 Figures 21A and 21B illustrate segmented teeth from a CBCT volume in a case where companion teeth are excluded for a missing tooth. The segmentation results are shown in an image 2402. The computed axes of inertia systems for the upper and lower jaws are in parallel as demonstrated in a graph 2404.

15 Figures 22A and 22B show the method of exclusion of companion teeth applied to another patient using tooth exclusion step S124 (Figure 2). As shown in an image 2500, teeth 2502, 2504, 2506 and 2508 are not fully developed. Their positioning, size, and orientation severely distort the physical properties of the upper jaw and lower jaw in terms of inertia system computation. 20 A graph 2510 in Fig 22B depicts the situation where upper jaw inertia system 2512 and lower jaw inertia system 2514 are severely misaligned (not in parallel).

25 Figures 23A and 23B show the results of excluding specific teeth from the image. An image 2600 shows the results of excluding teeth 2502, 2504, 2506 and 2508 from image 2500 of Figure 22A. Without the disturbance of these teeth, the axes of inertia system 2612 of the upper jaw and inertia system 2614 lower jaw of the teeth shown in image 2600 are in parallel as depicted in a graph 2610.

#### Biometry Computation

Given the entered landmark data for anatomic reference points, 30 segmentation of dentition elements such as teeth, implants, and jaws and related support structures, and the computed parameters obtained as described previously, detailed biometry computation can be performed and its results used to assist

setup of a treatment plan and monitoring ongoing treatment progress. Referring back to Figure 8, the biometry computation described subsequently gives more details about step S250 for analyzing and displaying parameters generated from the recorded reference marks.

5 According to an embodiment of the present disclosure, the entered landmarks and computed inertia systems of teeth are transformed from the original CBCT image voxel space to an alternate reference system, termed the direct orthogonal landmark (DOL) reference system, with coordinates  $(x_d, y_d, z_d)$ . Figure 24 shows a number of landmarks and coordinate axes or vectors of the  
 10 DOL reference system. Landmarks RIO and LIO indicate the infraorbital foramen; landmarks RHM and LHM mark the malleus. The origin  $\mathbf{0}_d$  of  $(\mathbf{x}_d, \mathbf{y}_d, \mathbf{z}_d)$  is selected at the middle of the line connecting landmarks RIO and LIO. Vector  $\mathbf{x}_d$  direction is defined from landmark RIO to LIO. A YZ plane is orthogonal to vector  $\mathbf{x}_d$  at point  $\mathbf{0}_d$ . There is an intersection point  $\mathbf{0}'_d$  of plane  
 15 YZ and the line connecting RHM and LHM. Vector  $\mathbf{y}_d$  direction is from  $\mathbf{0}'_d$  to  $\mathbf{0}_d$ . Vector  $\mathbf{z}_d$  is the cross product of  $\mathbf{x}_d$  and  $\mathbf{y}_d$ .

Using this transformation, the identified landmarks can be re-mapped to the coordinate space shown in Figure 25. Figure 26 shows, from a side view, an example with transformed inertia systems using this re-mapping.

20 By way of example, and not of limitation, the following listing identifies a number of individual data parameters that can be calculated and used for further analysis using the transformed landmark, dentition segmentation, and inertial system data.

25 A first grouping of data parameters that can be calculated using landmarks in the transformed space gives antero-posterior values:

1. Antero-posterior.alveolar.GIM-Gim: y position difference between the mean centers of inertia of upper and lower incisors.
2. Antero-posterior.alveolar.GM-Gm: difference between the mean centers of inertia of upper and lower teeth.

- 3. Antero-posterior.alveolar.TqIM: mean torque of upper incisors.
- 4. Antero-posterior.alveolar.Tqim: mean torque of lower incisors.
- 5. Antero-posterior.alveolar.(GIM+Gim)/2: average y position of GIM and Gim.
- 6. Antero-posterior.basis.MNP-MM: y position difference between mean nasal palatal and mean mental foramen.
- 7. Antero-posterior.basis.MFM-MM: actual distance between mean mandibular foramen and mean mental foramen.
- 8. Antero-posterior.architecture.MMy: y position of mean mental foramen.
- 9. Antero-posterior.architecture.MHM-MM: actual distance between mean malleus and mean mental foramen.

A second grouping gives vertical values:

- 10. Vertical.alveolar.Gdz: z position of inertial center of all teeth.
- 11. Vertical.alveolar.MxII-MdII: difference between the angles of second axes of upper and lower arches.
- 12. Vertical.basis.<MHM-MIO,MFM-MM>: angle difference between the vectors MHM-MIO and MFM-MM.
- 13. Vertical. architecture.MMz: z position of mean mental foramen.
- 14. Vertical. architecture.13: angle difference between the vectors MHM-MIO and MHM-MM.

Transverse values are also provided:

- 15. Transverse.alveolar.dM-dm: difference between upper right/left molars distance and lower right/left molars distance
- 16. Transverse.alveolar.TqM-Tqm: difference between torque of upper 1<sup>st</sup> & 2<sup>nd</sup> molars and torque of lower 1<sup>st</sup> & 2<sup>nd</sup> molars.
- 17. Transverse.basis.(RGP-LGP)/(RFM-LFM): ratio of right/left greater palatine distance and mandibular foramen distance.
- 18. Transverse.architecture.(RIO-LIO)/(RM-LM): ratio of right/left infraorbital foramen and mental foramen distances.

Other calculated or "deduced" values are given as follows:

- 19. Deduced.hidden.GIM: mean upper incisors y position.
- 20. Deduced.hidden.Gim: mean lower incisors y position.

21. Deduced.hidden.(TqIM+Tqim)/2: average of mean torque of upper incisors and mean torque of lower incisors.
22. Deduced.hidden.TqIM-Tqim: difference of mean torque of upper incisors and mean torque of lower incisors.
- 5 23. Deduced.hidden.MNPy: mean nasal palatal y position.
24. Deduced.hidden.GIM-MNP(y): difference of mean upper incisors y position and mean nasal palatal y position.
25. Deduced.hidden.Gim-MM(y): mean mental foramen y position.
26. Deduced.hidden.Gdz/(MMz-Gdz): ratio between value of Gdz and 10 value of MMz-Gdz.

It should be noted that this listing is exemplary and can be enlarged, edited, or changed in some other way within the scope of the present disclosure.

In the exemplary listing given above, there are 9 parameters in the 15 anterior-posterior category, 5 parameters in the vertical category and 4 parameters in the transverse category. Each of the above categories, in turn, has three types: alveolar, basis, and architectural. Additionally, there are 8 deduced parameters that may not represent a particular spatial position or relationship but that are used in subsequent computation. These parameters can be further labeled as normal or 20 abnormal.

Normal parameters have a positive relationship with anterior-posterior disharmony, that is, in terms of their values:

Class III < Class I < Class II.

wherein Class I values indicate a normal relationship between the upper teeth, 25 lower teeth and jaws or balanced bite; Class II values indicate that the lower first molar is posterior with respect to the upper first molar; Class III values indicate that the lower first molar is anterior with respect to the upper first molar.

Abnormal parameters have a negative relationship with anterior-posterior disharmony, that is, in terms of their bite-related values:

30 Class II < Class I < Class III.

Embodiments of the present disclosure can use an analysis engine in order to compute sets of probable conditions that can be used for interpretation

and as guides to treatment planning. Figures 27 - 38 show various aspects of analysis engine operation and organization and some of the text, tabular, and graphical results generated by the analysis engine. It should be noted that a computer, workstation, or host processor can be configured as an analysis engine 5 according to a set of preprogrammed instructions that accomplish the requisite tasks and functions.

According to an embodiment of the present disclosure, an analysis engine can be modeled as a three-layer network 2700 as shown in Figure 27. In this model, row and column node inputs can be considered to be directed to a set 10 of comparators 2702 that provide a binary output based on the row and column input signals. One output cell 2704 is activated for each set of possible input conditions, as shown. In the example shown, an input layer 1 2710 is fed with one of the 26 parameters listed previously and an input layer 2 2720 is fed with another one of the 26 parameters. An output layer 2730 contains 9 cells each one 15 of which represents one probable analysis if the two inputs meet certain criterion, that is, when their values are within particular ranges.

According to an embodiment of the present disclosure, the analysis engine has thirteen networks. These include independent networks similar to that shown in Figure 27 and coupled networks 2800 and 2810 as shown in Figure 28.

20 An algorithm shown in Figure 29 describes the operation of an independent analysis network, such as that shown in the example of Figure 27. Here, values  $x$  and  $y$  are the input parameter values;  $m$  represents the network index;  $\mathbf{D}(i,j)$  is the output cell. The steps of “evaluate vector  $\mathbf{c}_m$ ” for column values and “evaluate vector  $\mathbf{r}_m$ ” for row values check to determine what 25 evaluation criterion the input values meet. For example, in the following formula, if  $-\infty < x_m \leq \mu_{x_m}$  then  $\mathbf{c}_m = [\text{true}, \text{false}, \text{false}]$ .

The coupled network of Figure 28 combines results from two other networks and can operate as described by the algorithm in Figure 30. Again, values  $x$  and  $y$  are the input values;  $m$  represents the network index;  $\mathbf{D}(i,j)$  is the 30 output cell. The steps of “evaluate vector  $\mathbf{c}_k$ ” for column values and “evaluate

vector  $r_k$ " for row values check to determine what evaluation criterion the input values meet.

In a broader aspect, the overall arrangement of networks using the independent network model described with reference to Figure 27 or the coupled 5 network model described with reference to Figure 28 allow analysis to examine, compare, and combine various metrics in order to provide useful results that can be reported to the practitioner and used for treatment planning.

Figure 31A lists, for a particular patient, example parameters as numerical values and their interpretation with respect mainly to malocclusion of 10 teeth, based on the listing of 26 parameters given previously. Figures 31B, 31C and 31D list, for a particular patient, example parameters as numerical values and their interpretation with respect to maxilofacial asymmetry, based on the listing of total 63 parameters given in an exemplary embodiment of this application. Figure 32A shows exemplary tabulated results 3200 for a particular example with bite 15 analysis and arches angle characteristics. In the example of Figure 32A, the columns indicate an underjet, normal incisors relation, or overjet condition. Rows represent occlusal classes and arches angle conditions. As Figure 32A shows, highlighting can be used to accentuate the display of information that indicates an abnormal condition or other condition of particular interest. For the particular 20 patient in the Figure 32A example, analysis indicates, as a result, an underjet condition with Class III bite characteristics. This result can be used to drive treatment planning, depending on severity and practitioner judgment.

Figure 32B shows exemplary tabulated results 3200 for another example with analysis of torque for upper and lower incisors, using parameters 3 25 and 4 from the listing given previously.

Figure 32C shows exemplary tabulated results 3200 for another example with assessment of biretrusion or biprotrusion using calculated parameters given earlier as parameters (5) and (21).

Figure 32D shows an exemplary summary listing of results for 30 cephalometric analysis of a particular patient. The listing that is shown refers to analysis indications taken relative to parameters 1 - 26 listed previously. In the particular example of Figure 32D, there are 13 results for parameter comparisons

using biometric parameters and dentition information derived as described herein. Additional or fewer results could be provided in practice. Figure 32E shows a detailed listing for one of the conditions reported in a tabular listing with a table 3292 with cells 3294 as shown subsequently (Figure 35).

5                   Results information from the biometry computation can be provided for the practitioner in various different formats. Tabular information such as that shown in Figures 31A - 32E can be provided in file form, such as in a comma-separated value (CSV) form that is compatible for display and further calculation in tabular spreadsheet arrangement, or may be indicated in other 10 forms, such as by providing a text message. A graphical display, such as that shown in Figure 26, can alternately be provided as output, with particular results highlighted, such as by accentuating the intensity or color of the display for features where measured and calculated parameters show abnormal biometric relations, such as overjet, underjet, and other conditions.

15                  The computed biometric parameters can be used in an analysis sequence in which related parameters are processed in combination, providing results that can be compared against statistical information gathered from a patient population. The comparison can then be used to indicate abnormal relationships between various features. This relationship information can help to show how 20 different parameters affect each other in the case of a particular patient and can provide resultant information that is used to guide treatment planning.

Referring back to Figure 1, memory 132 can be used to store a statistical database of cephalometric information gathered from a population of patients. Various items of biometric data that provides dimensional information 25 about teeth and related supporting structures, with added information on bite, occlusion, and interrelationships of parts of the head and mouth based on this data can be stored from the patient population and analyzed. The analysis results can themselves be stored, providing a database of predetermined values capable of yielding a significant amount of useful information for treatment of individual 30 patients. According to an embodiment of the present disclosure, the parameter data listed in Figures 31A and 31B are computed and stored for each patient, and may be stored for a few hundred patients or for at least a statistically significant

group of patients. The stored information includes information useful for determining ranges that are considered normal or abnormal and in need of correction. Then, in the case of an individual patient, comparison between biometric data from the patient and stored values calculated from the database can 5 help to provide direction for an effective treatment plan.

As is well known to those skilled in the orthodontic and related arts, the relationships between various biometric parameters measured and calculated for various patients can be complex, so that multiple variables must be computed and compared in order to properly assess the need for corrective action.

10 The analysis engine described in simple form with respect to Figures 27 and 28 compares different pairs of parameters and provides a series of binary output values. In practice, however, more complex processing can be performed, taking into account the range of conditions and values that are seen in the patient population.

15 Highlighting particular measured or calculated biometric parameters and results provides useful data that can guide development of a treatment plan for the patient.

Figure 33 shows a system display of results 3200 with a recommendation message 170 based on analysis results and highlighting features 20 of the patient anatomy related to the recommendation. Figure 34 shows a system display 108 with a graphical depiction of analysis results 3200. Annotated 3-D views (e.g., 308a-308d) are shown, arranged at different angles, along with recommendation message 170 and controls 166.

Certain exemplary method and/or apparatus embodiments 25 according to the present disclosure can address the need for objective metrics and displayed data that can be used to help evaluate asymmetric facial/dental anatomic structure. Advantageously, exemplary method and/or apparatus embodiments present measured and analyzed results displayed in multiple formats suitable for assessment by the practitioner.

30 Figure 35 shows an exemplary text report for maxillofacial asymmetry assessment according to an embodiment of the present disclosure. The report lists a set of assessment tables (T1 - T19) available from the system, with

cell entries (denoted by C with row and column indices, C(row, column)) providing maxillofacial/dental structural asymmetry property assessment comments organized based on the calculations related to relationships between obtained parameters, such as parameters P1-P15 in Figure 31B. An exemplary 5 assessment table 3292 is depicted in Figure 32E, having four rows and four columns.

In one embodiment, for each exemplary assessment table (e.g., 19 assessment tables), only one cell 3294 can be activated at a time; the activated cell content is highlighted, such as by being displayed in red font. In the exemplary 10 table 3292, the activated cell is C(2,2) (3294) with a content “0” indicating that asymmetry is not found for the property of incisors and molars upper/lower deviations.

For a quick reference to the exemplary assessment tables, the system of the present disclosure generates a checklist type concise summary page 15 (e.g., Figure 35) that provides information with respect to table numbers ( $T_n$ ), parameter numbers ( $P_k, j$ ), cell indices ( $C_s, t$ ), and actual assessment comments from assessment tables T1-T19. The information obtained from this type of text report can be helpful for the practitioner, providing at least some objective metrics that can be useful in developing a treatment plan for a particular patient or 20 evaluating treatment progress. Further beneficial to the practitioner can be cumulative summative evaluations directed to overall condition assessments of a patient. This can be the situation, in particular, when numbers of conditional reference points and relationships therebetween utilized to determine asymmetric facial/dental anatomic structures or relationships for a patient involve large 25 numbers of view-oriented and 3D-oriented treatment conditions, with variable underlying causes.

In one exemplary asymmetric determination table embodiment, 19 assessment tables can be included with hundreds of reference points and several hundreds of relationships therebetween. In this exemplary asymmetric 30 determination table embodiment, tables include: T1: Asymmetric matching incisors and molars upper/lower deviations; T2: Arch rotation; T3: Upper/lower arch right rotation and upper or lower arch responsibility; T4: Asymmetric

matching incisors upper/lower deviations with upper inc transverse deviation, response of upper or lower arch in the upper/lower incisors trans deviation; T5: Asymmetric matching incisors upper/lower deviations with anterior bases transverse deviation, response of upper or lower arch anterior deviation in the

5 upper/lower incisors trans deviation; T6: Asymmetric matching incisors upper/lower molar deviations with upper molars transverse deviation, response of upper or lower molars trans deviation; T7: Asymmetric matching incisors upper/lower molar deviations with lower molars transverse deviation; T8: Asymmetric matching basic bones upper/lower deviations; T9: Asymmetric

10 matching basic bones upper/lower anterior relations with anterior maxilla deviation; T10: Asymmetric matching basic bones upper/lower anterior relations with anterior mandible deviation; T11: Asymmetric matching incisors upper/lower deviations with anterior bases transverse deviation; T12: Vertical asymmetric comparing L/R molars altitudes difference with maxillary arch rolling; T13:

15 Asymmetric comparing L/R molars altitudes difference with mandible arch rolling; T14: Vertical asymmetric comparing basic bones R/L posterior differences (maxillary & mandible); T15: Vertical asymmetric comparing L/R difference at mental points level (measuring maxilla-facial area and global face); T16: Anterior-posterior asymmetric comparing R/L upper/lower molars anterior-posterior difference with lower ones; T17: Anterior-posterior asymmetric comparing R/L upper/lower molars anterior-posterior relationship difference with lower ones; T18: Anterior-posterior asymmetric comparing L/R upper basis lateral landmarks anterior-posterior difference with lower ones; T19: Anterior-posterior asymmetric matching mandibular horizontal branch with R/L global hemifaces;

20

25 In such complex asymmetric facial/dental anatomic structures or relationships determinations according to this application, optional cumulative summative evaluations directed to overall condition assessments of a patient are preferably used. In some embodiments, exemplary cumulative summative or overall diagnosis comments can include: Asymmetry anterior posterior direction (AP comment or S1), Asymmetry vertical direction (VT comment or S2), and Asymmetry Transverse direction (TRANS comment or S3). Still further, highest level evaluation score(s) can be used by using one or more or combining S1, S2

30

and S3 to determine an Asymmetry global score (Asymmetry Global determination). For example, the exemplary Asymmetry global score can be a summary (e.g., overall class I, II, III), broken into few, limited, categories (e.g., normal, limited evaluation, detailed assessment suggested) or  
5 represented/characterized by dominant asymmetry condition (e.g., S1, S2, S3).

As shown in Figure 35, the exemplary text report also presents S1 anterior-posterior direction “synthetic” asymmetry comment, S2 vertical direction synthetic asymmetry comment, and S3 transversal direction synthetic asymmetry comment.

10 The “synthetic” terminology is derived in this application to from a pair of tables in each direction. In certain exemplary embodiments, the “synthetic” terminology can be determined from a combination of a plurality of tables from each assessment type (e.g., AP, V, Trans involving or representing substantial (e.g., >50%) portions of the skull) or a pair of tables in each direction.

15 For example, S1 synthetic comment is derived from Table 17 and Table 19. The derivation first assigns a score to each of the cells of Table 17 and Table 19. An exemplary score assignment is explained as follows

For Table 17,  $C(1,3) = -2$ ;  $C(1,2) = C(2,3) = -1$ ;  $C(2,1) = C(3,2) = 1$ ;  $C(3,1) = 2$ ; other cells are assigned with a value 0.

20 For Table 19,  $C(1,1) = -2$ ;  $C(1,2) = C(2,1) = -1$ ;  $C(2,3) = C(3,2) = 1$ ;  $C(3,3) = 2$ ; other cells are assigned with a value 0.

The derivation of S1 synthetic comment evaluates the combined score by adding the scores from Table 17 and Table 19.

25 For instance, if  $C(1,3)$  in Table 17 is activated and  $C(1,1)$  in Table 19 is activated then the combined score will be the summation of the scores of  $C(1,3)$  of Table 17 and  $C(1,1)$  of Table 19. Since  $C(1,3)$  in Table 17 is assigned with a value -2 and  $C(1,1)$  in Table 19 is assigned with a value -2, therefore, the combined the score is -4. Obviously, the possible combined sore values for S1 are -4, -3, -2, -1, 0, 1, 2, 3 and 4.

30 The exemplary S1 synthetic comments can be based on the combined score value are summarized below.

If the combined score = -4 or -3, the S1 synthetic comment = strong left anterior-posterior excess.

If the combined score = -2, the S1 synthetic comment = left anterior-posterior excess tendency.

5 If the combined score = 2, the S1 synthetic comment = right anterior-posterior excess tendency.

If the combined score = 4 or 3, the S1 synthetic comment = strong right anterior-posterior excess.

If the combined score = 0, no comment.

10 Similar synthetic comment derivations are applied to the vertical direction and transversal direction.

Referring back to Figure 35, the exemplary text report displays S1 = strong right anteroposterior excess, S2 = none and S3 = left upper deviation tendency.

15 In very rare cases, synthetic comments show up in all three directions, or the comments present some type of mixture of synthetic comments, which can prompt further extended diagnosis and/or treatment.

20 Further, selected exemplary method and/or apparatus embodiments according to the application can also provide a quick visual assessment of the asymmetry property of the maxillofacial/dental structural of a patient.

25 Figure 36 is a plot or graph that shows the maxillofacial/dental structural features for a patient with respect to a front view, plotted using the landmarks, reference marks 414, selected by the operator (see Figure 5). This type of displayed plot clearly shows asymmetry (left vs. right) in an objective fashion for this exemplary patient.

Likewise, Figure 37 is a plot or graph of a sagittal view, with reference marks 414 showing how closely the left and right sides of a patient's face overlap, as another objective indicator of asymmetry.

30 Figure 38 is a plot or graph providing a quick visual assessment of noticeable improper alignment of the bite of a patient in a sagittal view of upper and lower jaw planes 704 and 702. Jaw plane 704 is computed based on the derived upper jaw marks 814, lower jaw plane 702 is computed based on the

derived lower jaw marks 814. Derived marks 814 are computed based on the segmented teeth 304 shown in Figure 4 and show the location of the tooth. The example shown in Figure 38 depicts exemplary visual cues for a patient with a hyperdivergent pattern.

5                   Described herein is a computer-executed method for 3-D cephalometric analysis of maxillofacial asymmetry for a patient. The method acquires and displays reconstructed volume image data from a computed tomographic scan of a patient's head from at least a first 2-D view. An operator instruction positions and displays at least one reference mark on the at least the 10 first displayed 2-D view. One or more dentition elements within the mouth of the patient are then segmented. The method computes and displays cephalometric parameters for the patient according to data from the at least one reference mark and the one or more segmented dentition elements and computes, using the computed cephalometric parameters, one or more results indicative of 15 maxillofacial asymmetry. The method then energizes a graphical or text display to show the computed results indicative of maxillofacial asymmetry.

                  Consistent with exemplary embodiments herein, a computer program can use stored instructions that perform 3D biometric analysis on image data that is accessed from an electronic memory. As can be appreciated by those 20 skilled in the image processing arts, a computer program for operating the imaging system and probe and acquiring image data in exemplary embodiments of the application can be utilized by a suitable, general-purpose computer system operating as control logic processors as described herein, such as a personal computer or workstation. However, many other types of computer systems can be 25 used to execute the computer program of the present invention, including an arrangement of networked processors, for example. The computer program for performing exemplary method embodiments may be stored in a computer readable storage medium. This medium may include, for example; magnetic storage media such as a magnetic disk such as a hard drive or removable device or magnetic 30 tape; optical storage media such as an optical disc, optical tape, or machine readable optical encoding; solid state electronic storage devices such as random access memory (RAM), or read only memory (ROM); or any other physical

device or medium employed to store a computer program. Computer programs for performing exemplary method embodiments may also be stored on computer readable storage medium that is connected to the image processor by way of the internet or other network or communication medium. Those skilled in the art will 5 further readily recognize that the equivalent of such a computer program product may also be constructed in hardware.

It should be noted that the term “memory”, equivalent to “computer-accessible memory” in the context of the application, can refer to any type of temporary or more enduring data storage workspace used for storing and 10 operating upon image data and accessible to a computer system, including a database, for example. The memory could be non-volatile, using, for example, a long-term storage medium such as magnetic or optical storage. Alternately, the memory could be of a more volatile nature, using an electronic circuit, such as random-access memory (RAM) that is used as a temporary buffer or workspace 15 by a microprocessor or other control logic processor device. Display data, for example, is typically stored in a temporary storage buffer that is directly associated with a display device and is periodically refreshed as needed in order to provide displayed data. This temporary storage buffer is also considered to be a type of memory, as the term is used in the application. Memory is also used as the 20 data workspace for executing and storing intermediate and final results of calculations and other processing. Computer-accessible memory can be volatile, non-volatile, or a hybrid combination of volatile and non-volatile types.

It will be understood that computer program products of the application may make use of various image manipulation algorithms and 25 processes that are well known. Additional aspects of such algorithms and systems, and hardware and/or software for producing and otherwise processing the images or co-operating with the computer program product exemplary embodiments of the application, are not specifically shown or described herein and may be selected from such algorithms, systems, hardware, components and 30 elements known in the art.

Certain exemplary method and/or apparatus embodiments according to the application can allow the practitioner to take advantage of

objective metrics and/or displayed data to help evaluate asymmetric facial/dental anatomic structure(s). Advantageously, exemplary method and/or apparatus embodiments can provide multiple graduated or hierarchical measured and analyzed results displayed in successively higher order formats suitable for

5 assessment by the practitioner. Although embodiments of the present disclosure are illustrated using dental imaging apparatus, similar principles can be applied for other types of diagnostic imaging and for other anatomy. Exemplary embodiments according to the application can include various features described herein (individually or in combination).

10 While the invention has been illustrated with respect to one or more implementations, alterations and/or modifications can be made to the illustrated examples without departing from the spirit and scope of the appended claims. In addition, while a particular feature of the invention can have been disclosed with respect to only one of several implementations/embodiments, such

15 feature can be combined with one or more other features of the other implementations/embodiments as can be desired and advantageous for any given or particular function. The term “at least one of” is used to mean one or more of the listed items can be selected. The term “about” indicates that the value listed can be somewhat altered, as long as the alteration does not result in

20 nonconformance of the process or structure to the illustrated embodiment.

Finally, “exemplary” indicates the description is used as an example, rather than implying that it is an ideal. Other embodiments of the invention will be apparent to those skilled in the art from consideration of the specification and practice of the invention disclosed herein. It is intended that the specification and examples

25 be considered as exemplary only, with a true scope and spirit of the invention being indicated by at least the following claims.

## CLAIMS

1. A method for 3-D cephalometric analysis of a patient, the method executed at least in part on a computer processor and comprising:
  - displaying reconstructed volume image data from a computed tomographic scan of a patient's head from at least a first 2-D view;
  - accepting an operator instruction that positions and displays at least one reference mark on the at least the first displayed 2-D view;
  - segmenting one or more dentition elements within the mouth of the patient;
  - computing and displaying a plurality of cephalometric parameters for the patient according to data from the at least one reference mark and the one or more segmented dentition elements;
  - computing, using the computed cephalometric parameters, one or more results indicative of maxillofacial asymmetry; and
  - energizing a graphical or text display to show the computed results indicative of maxillofacial asymmetry, where the display includes:
    - a first plurality of entries representing different selected maxillofacial asymmetric anterior posterior relations, asymmetry vertical relations and asymmetry transverse relations, and
    - a second plurality of entries representing synthesized maxillofacial asymmetric cumulative anterior posterior condition, cumulative asymmetry vertical condition, and cumulative asymmetry transverse condition, which are generated using the first plurality of entries.
2. The method of claim 1 wherein the plurality of cephalometric parameters graphically show asymmetry from a frontal view or a saggital view.
3. The method of claim 1 further comprising comparing the computed results with previously computed results and displaying a message related to the comparison.

4. The method of claim 1 further comprising displaying one or more of the reference marks on a second 2-D view that is substantially orthogonal to the first 2-D view.

5. The method of claim 1 wherein computing and displaying a plurality of cephalometric parameters comprises generating a three-dimensional framework related to the computed cephalometric parameters.

6. The method of claim 1 where showing the computed results comprises evaluating one or more of the computed results against a value calculated from a sampling of a patient population, and where the at least one reference mark identifies an anatomical feature that is outside the mouth of the patient.

7. The method of claim 1 further comprising generating and displaying a tabular report according to calculations from the computed cephalometric parameters for each of the first plurality of entries, where said each of the first plurality of entries correspond to a one active cell of cells in the tabular report corresponding thereto.

8. The method of claim 1 further comprising a third entry representing a combination of the synthesized maxillofacial asymmetric cumulative anterior posterior condition, the cumulative asymmetry vertical condition, and the cumulative asymmetry transverse condition.

9. The method of claim 1 further comprising displaying a graphical plot that shows the at least one reference mark and the computed results indicative of maxillofacial asymmetry.

10. The method of claim 9 where the displayed graphical plot shows computed results from a sagittal view, where the one or more results are indicative of tooth deviation. .

11. A logic processor that is configured with encoded instructions for:
  - displaying reconstructed volume image data from a computed tomographic scan of a patient's head from at least a first 2-D view;
  - segmenting one or more dentition elements within the mouth of the patient;
  - computing and displaying a plurality of cephalometric parameters for the patient according to data from at least one maxillofacial reference mark and the one or more segmented dentition elements;
  - computing, using the computed cephalometric parameters, one or more results indicative of maxillofacial asymmetry; and
  - energizing a graphical or text display to show the computed results indicative of asymmetry, energizing a graphical or text display to show the computed results indicative of maxillofacial asymmetry, where the display includes:
    - a first plurality of entries representing different selected maxillofacial asymmetric anterior posterior relations, asymmetry vertical relations and asymmetry transverse relations, and
    - a second plurality of entries representing synthesized maxillofacial asymmetric cumulative anterior posterior condition, cumulative asymmetry vertical condition, and cumulative asymmetry transverse condition, which are generated using the first plurality of entries.

12. The logic processor of claim 11 configured for cephalometric parameters using an analysis engine model having a plurality of networks.

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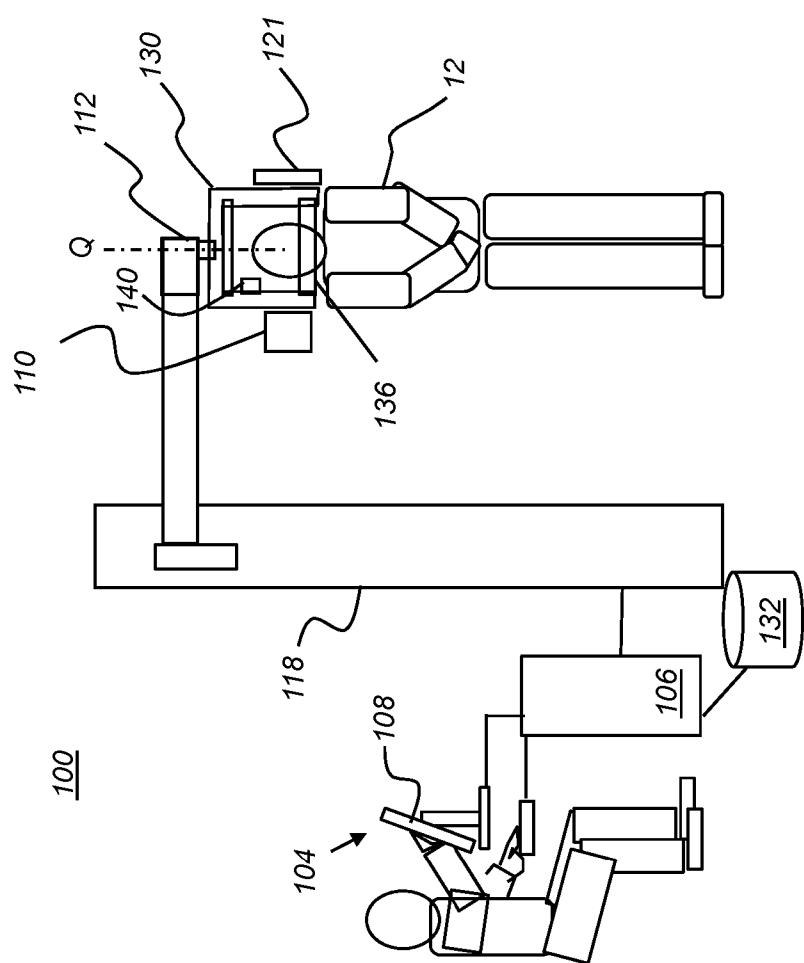
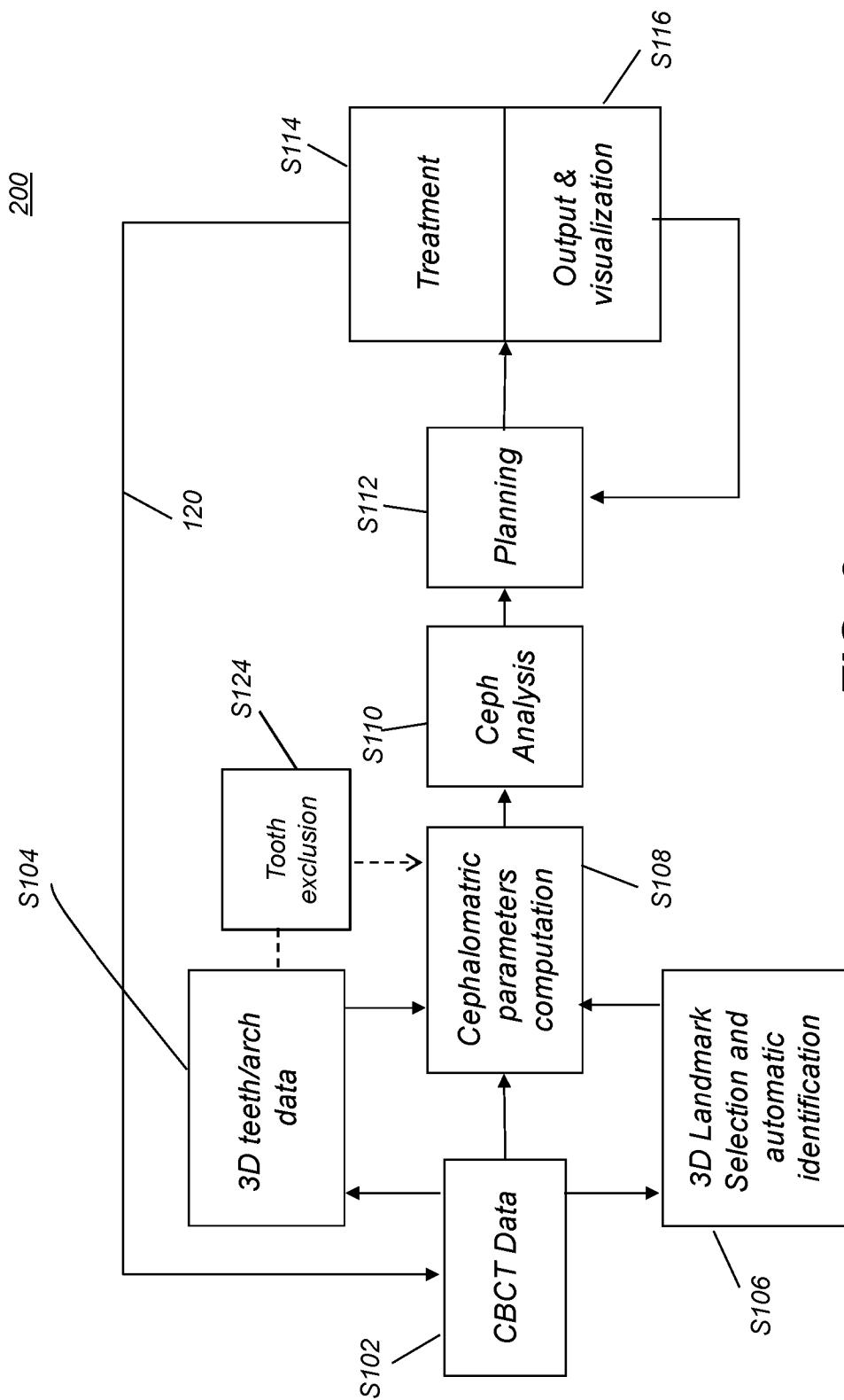


FIG. 1

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FIG. 3



FIG. 4

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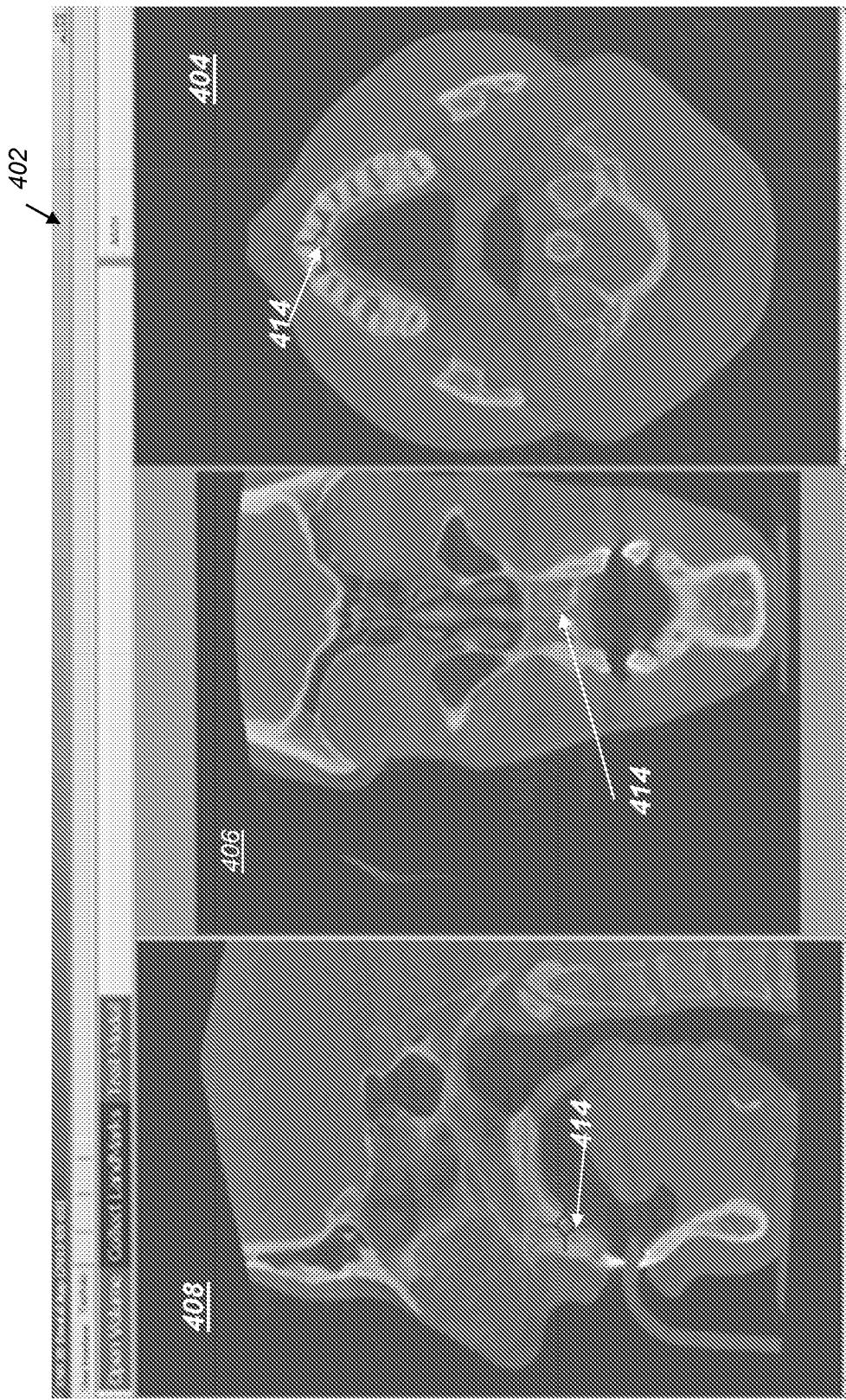


FIG. 5

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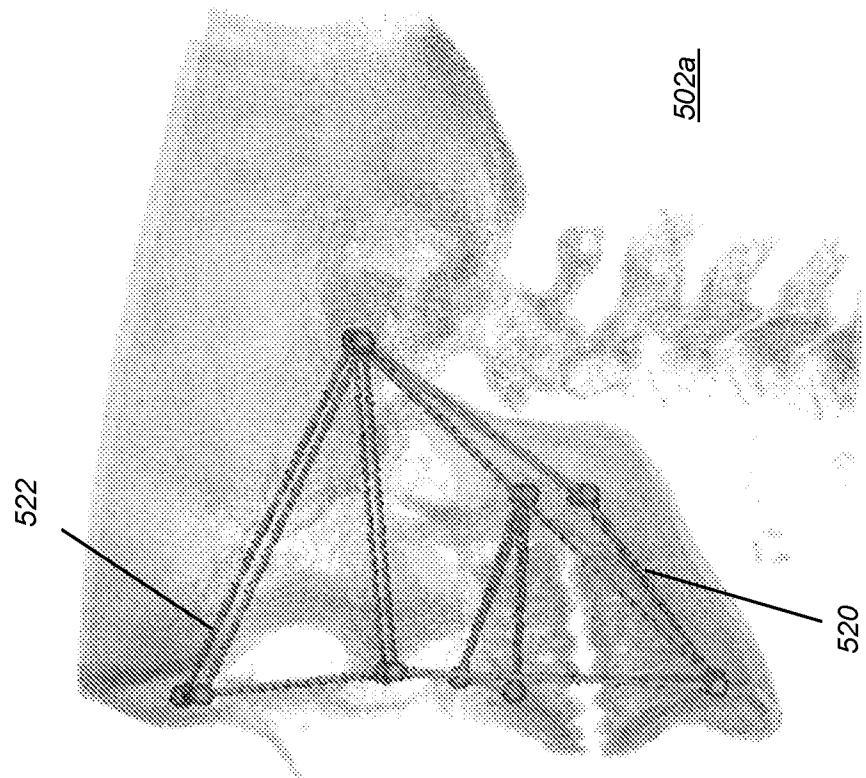


FIG. 7A

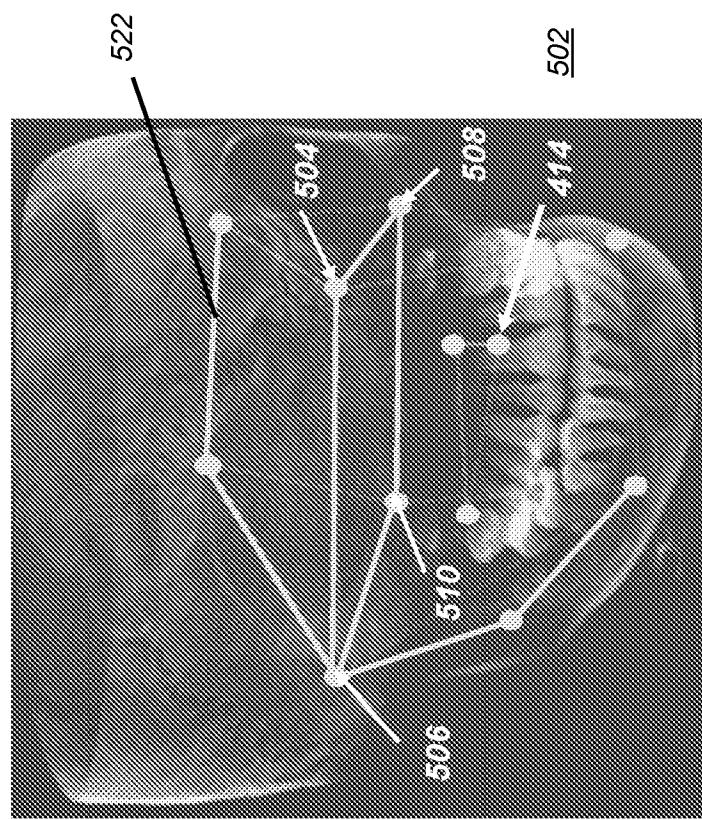


FIG. 6

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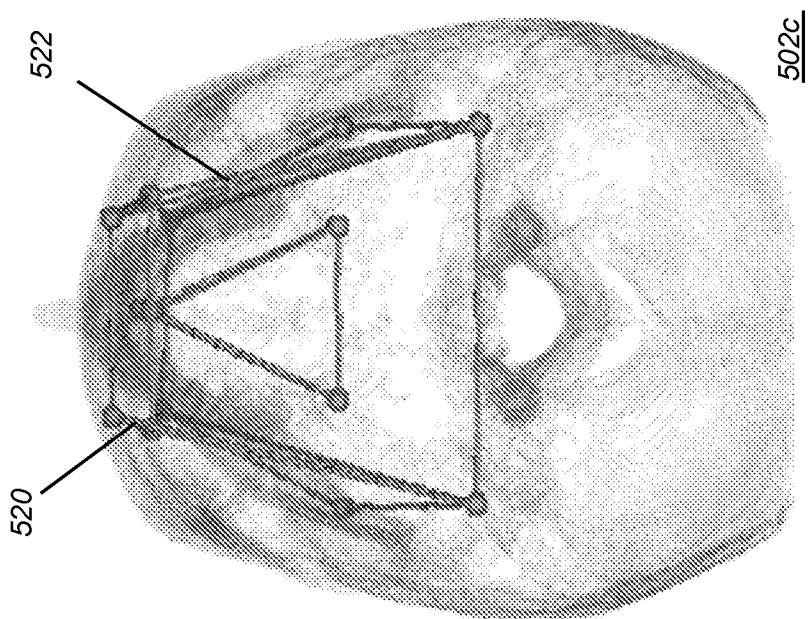


FIG. 7C

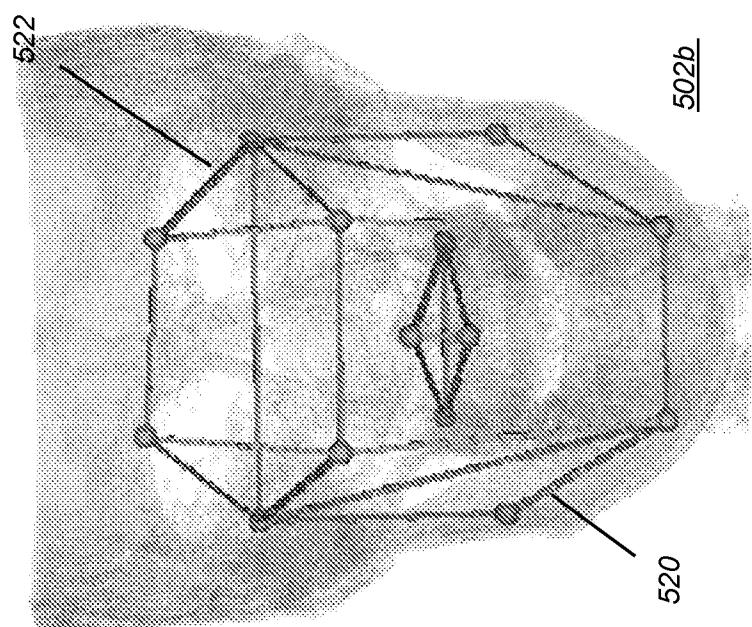
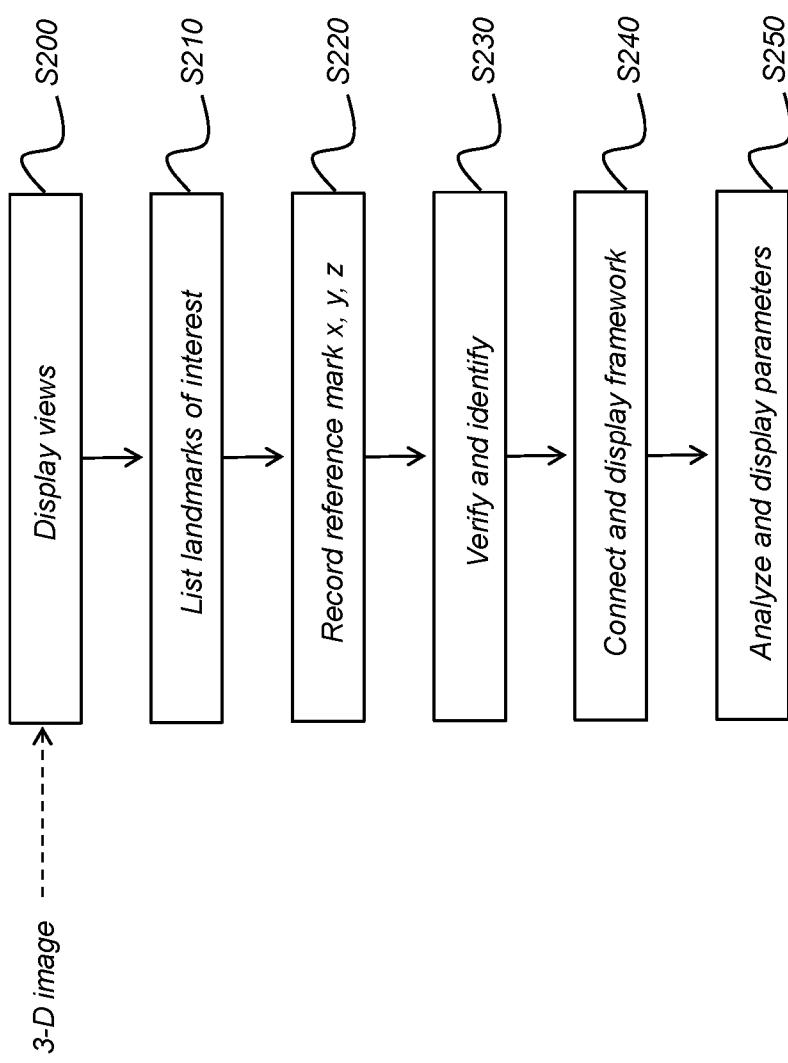


FIG. 7B

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**FIG. 8**

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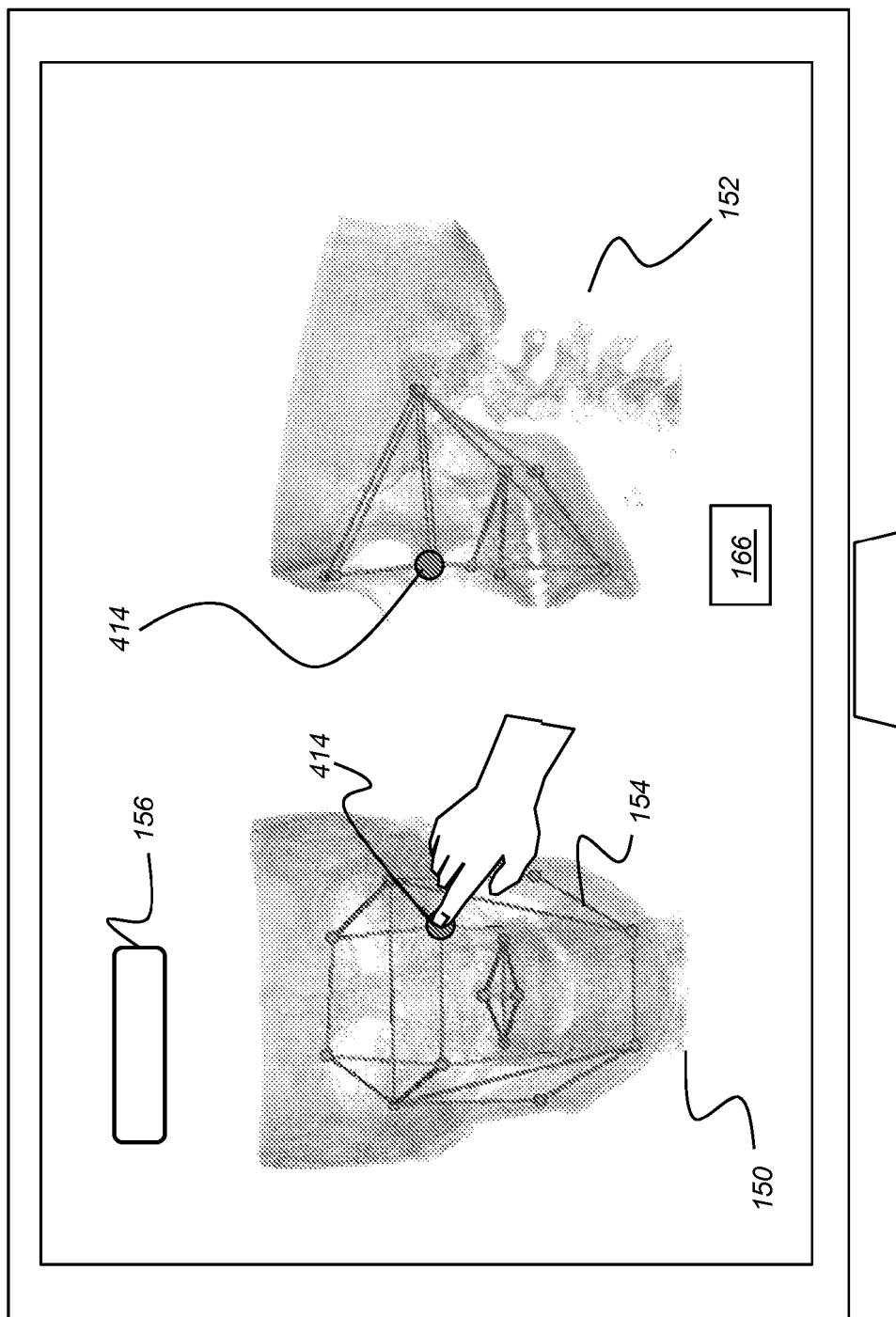
108

FIG. 9A

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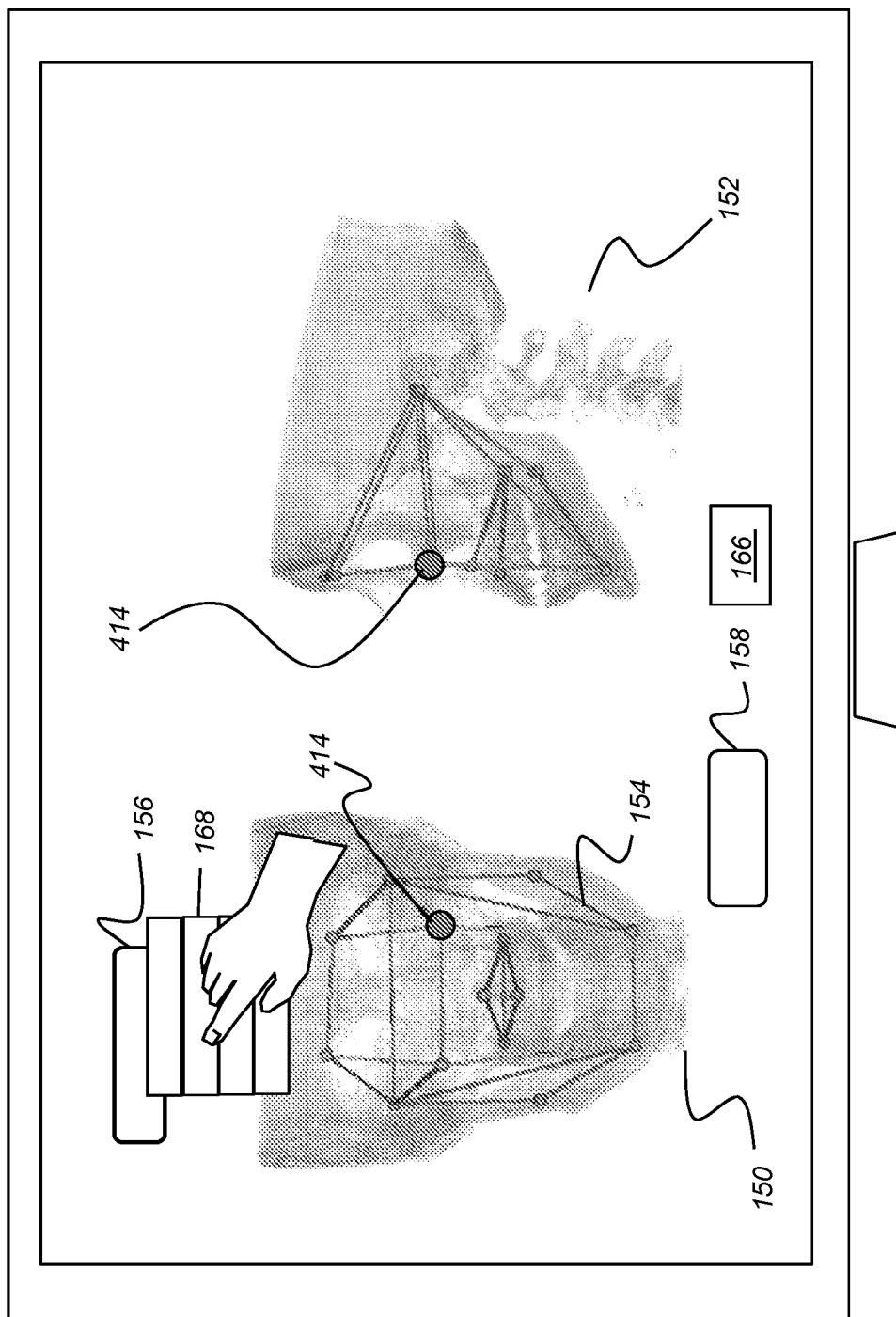
108

FIG. 9B

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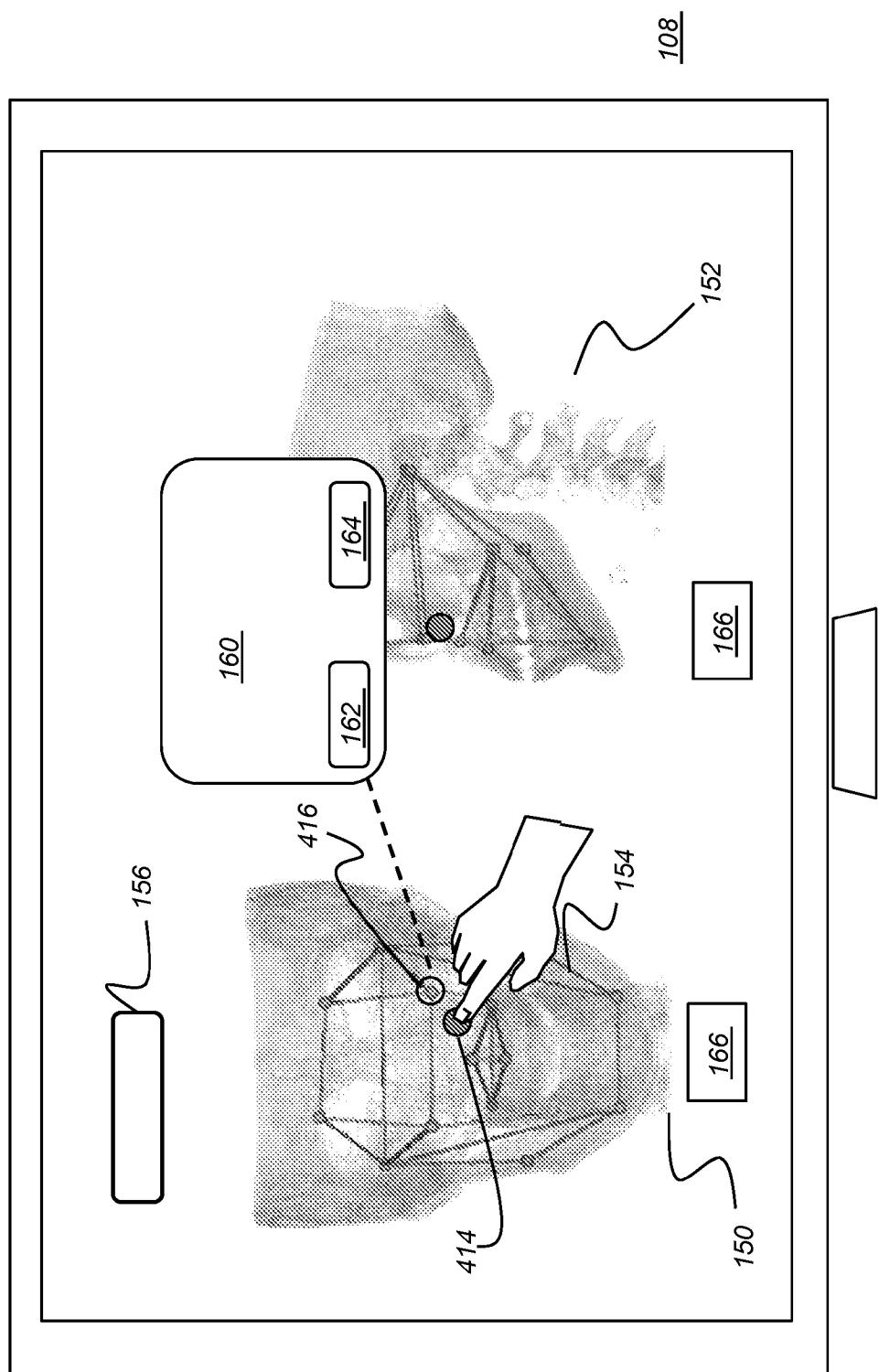


FIG. 9C

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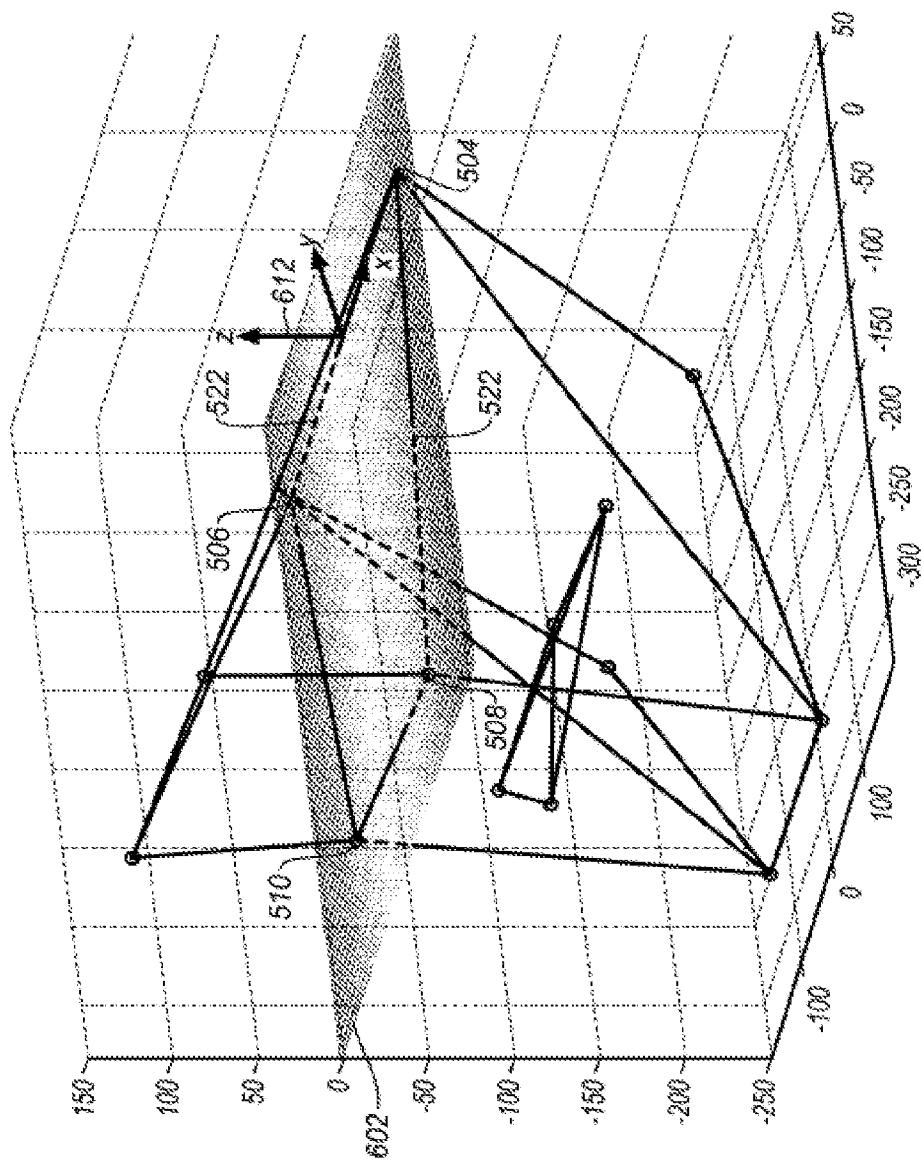
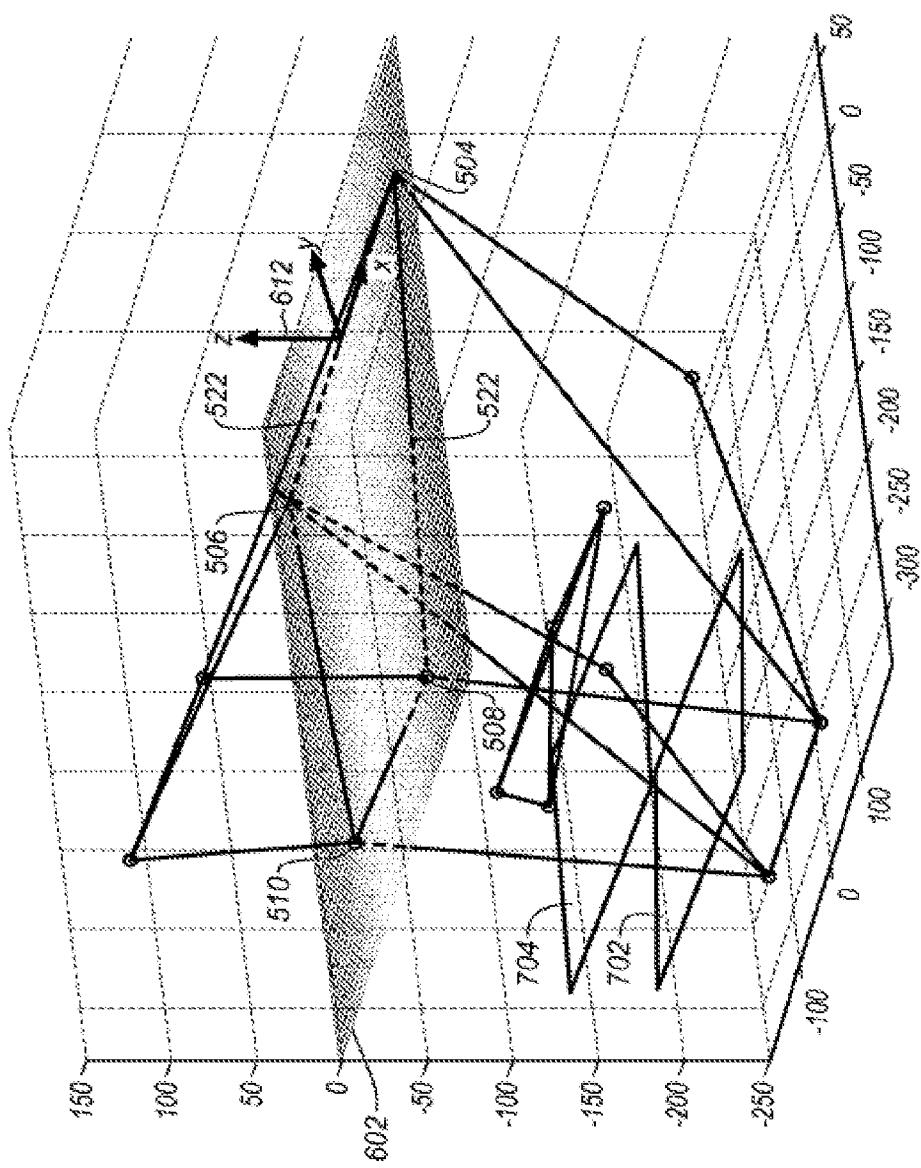


FIG. 10A

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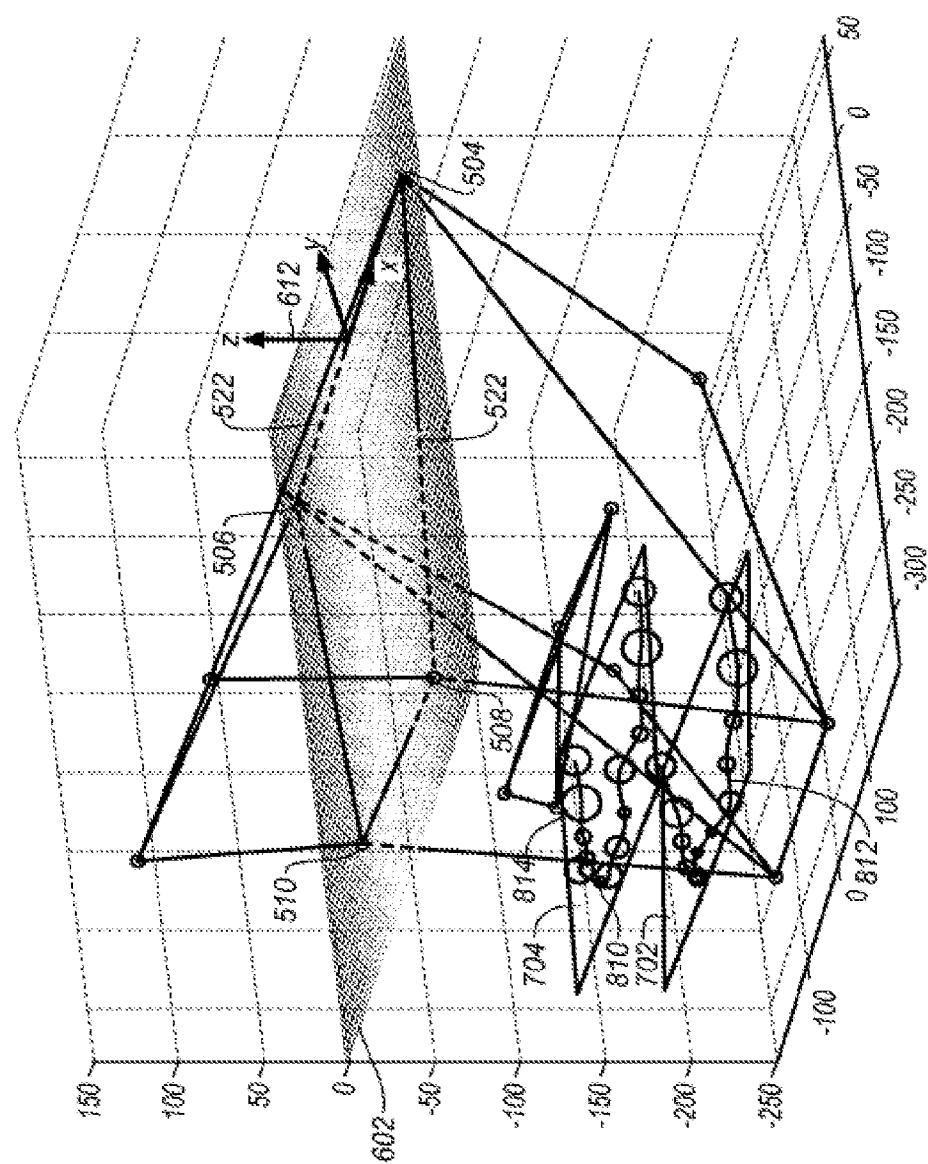


FIG. 10C

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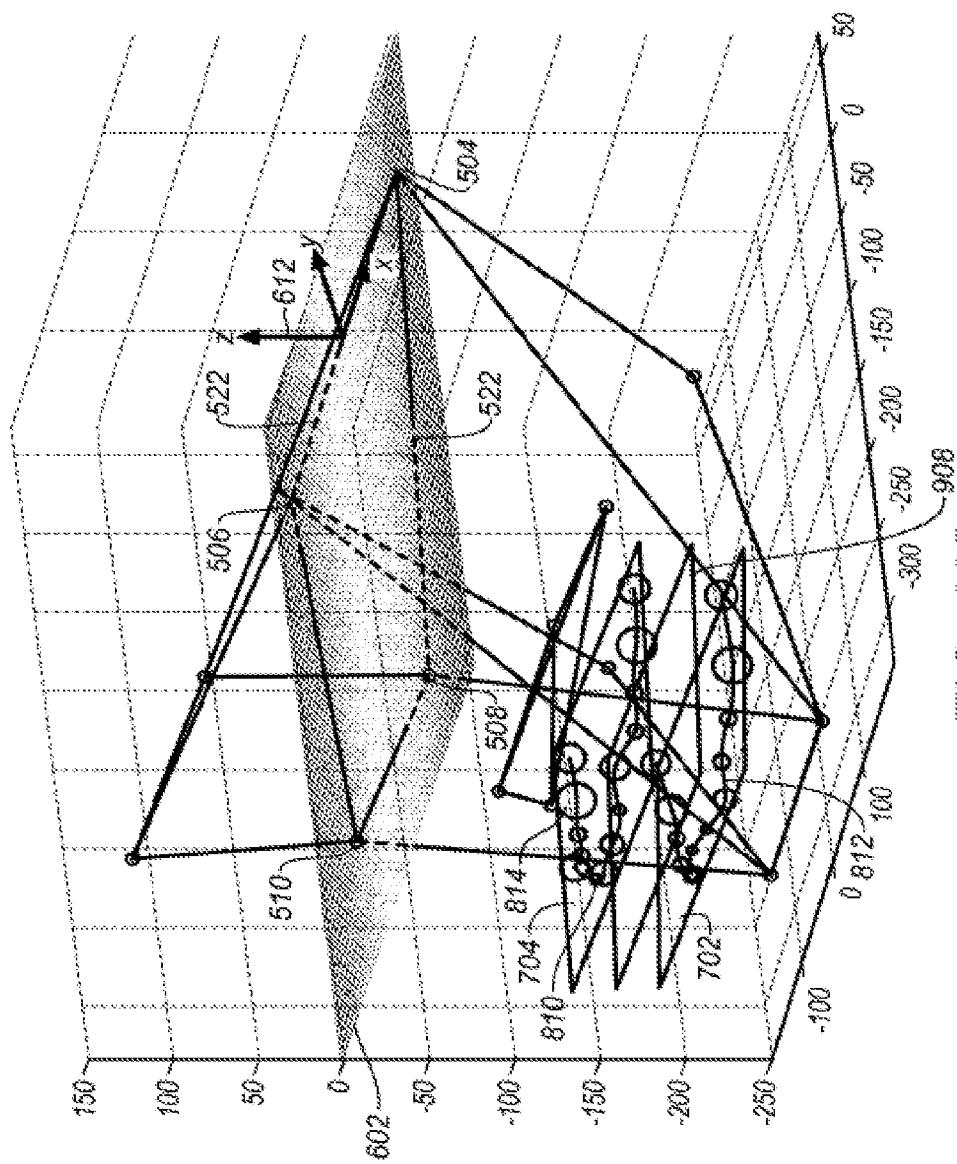
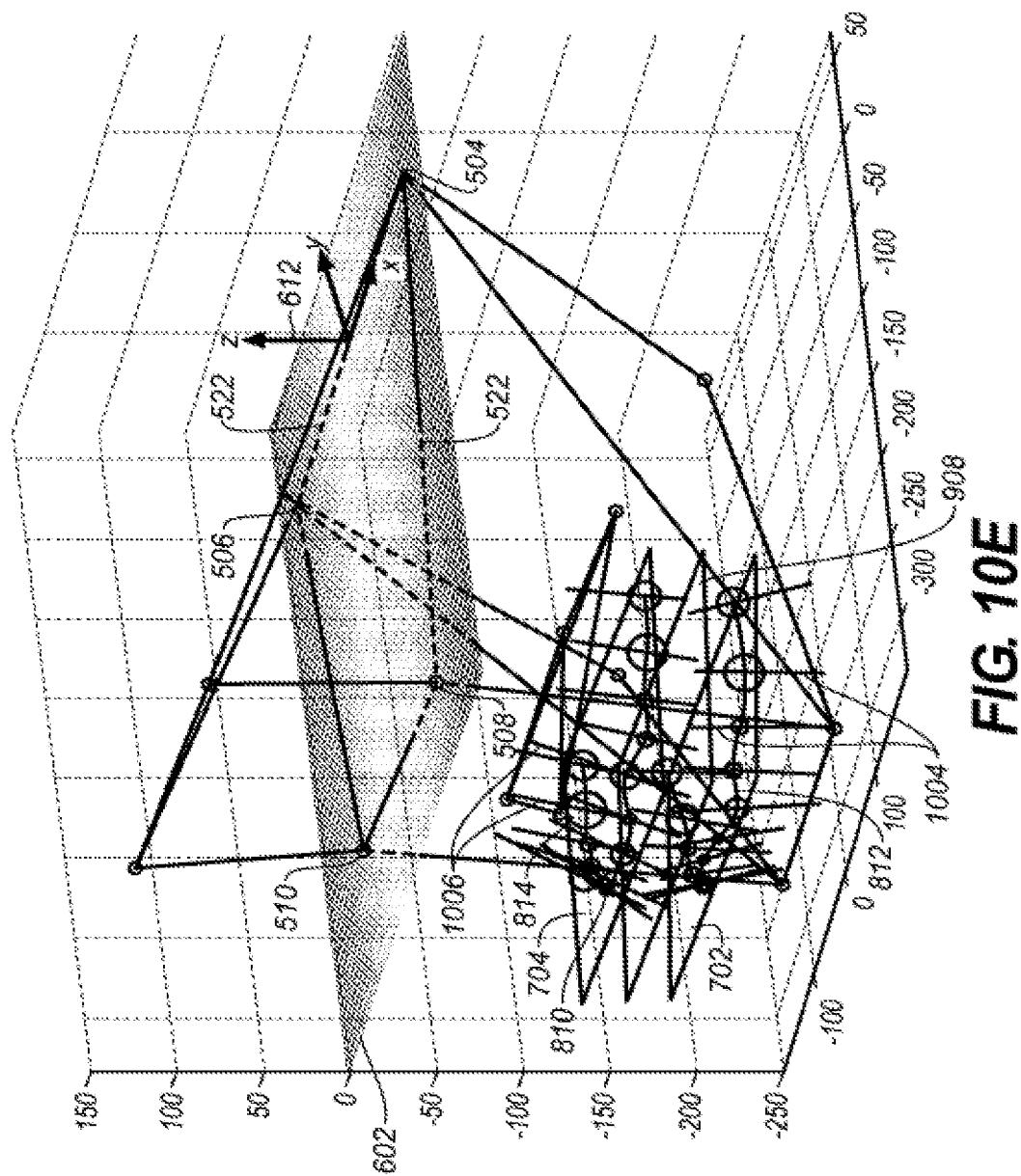


FIG. 10D

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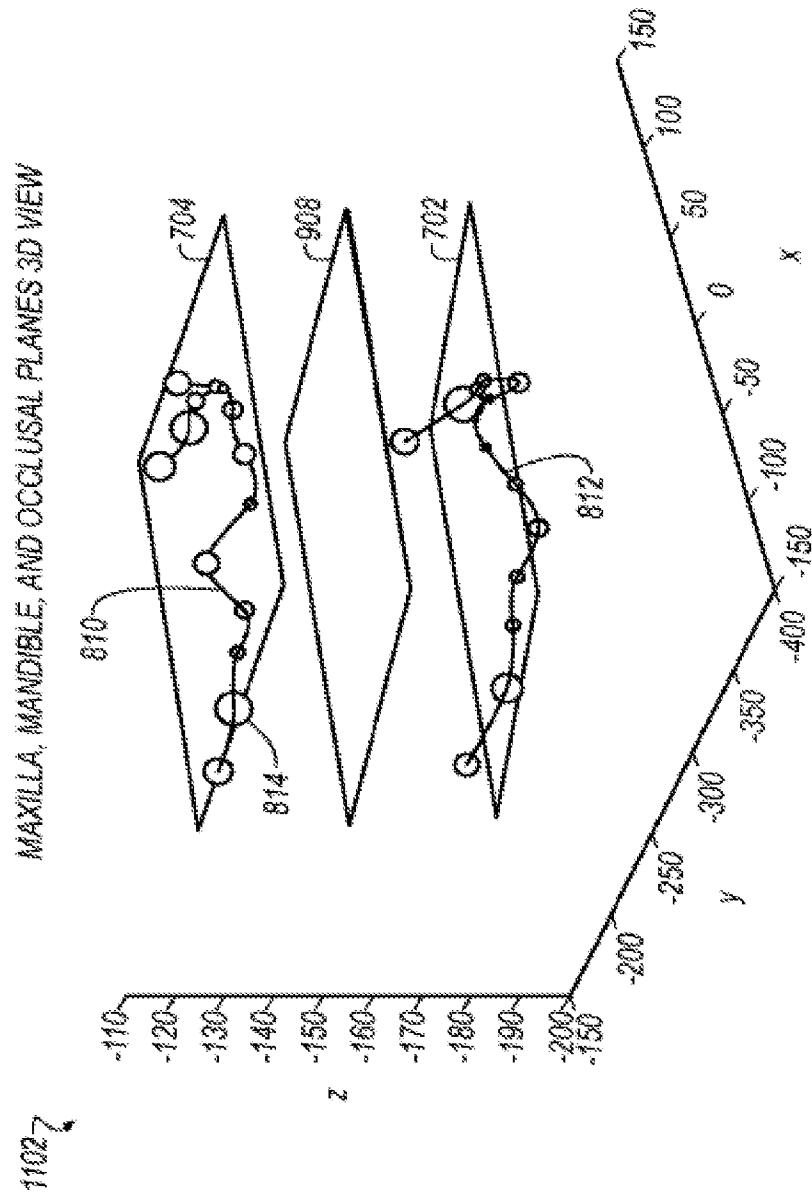


FIG. 11

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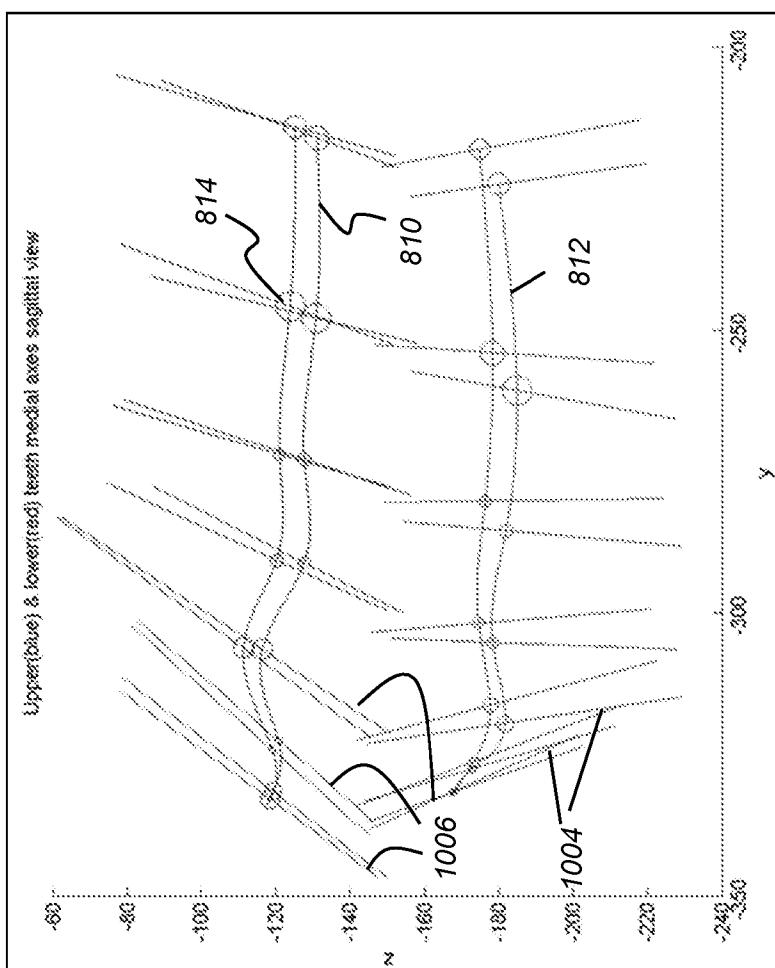
1202

FIG. 12

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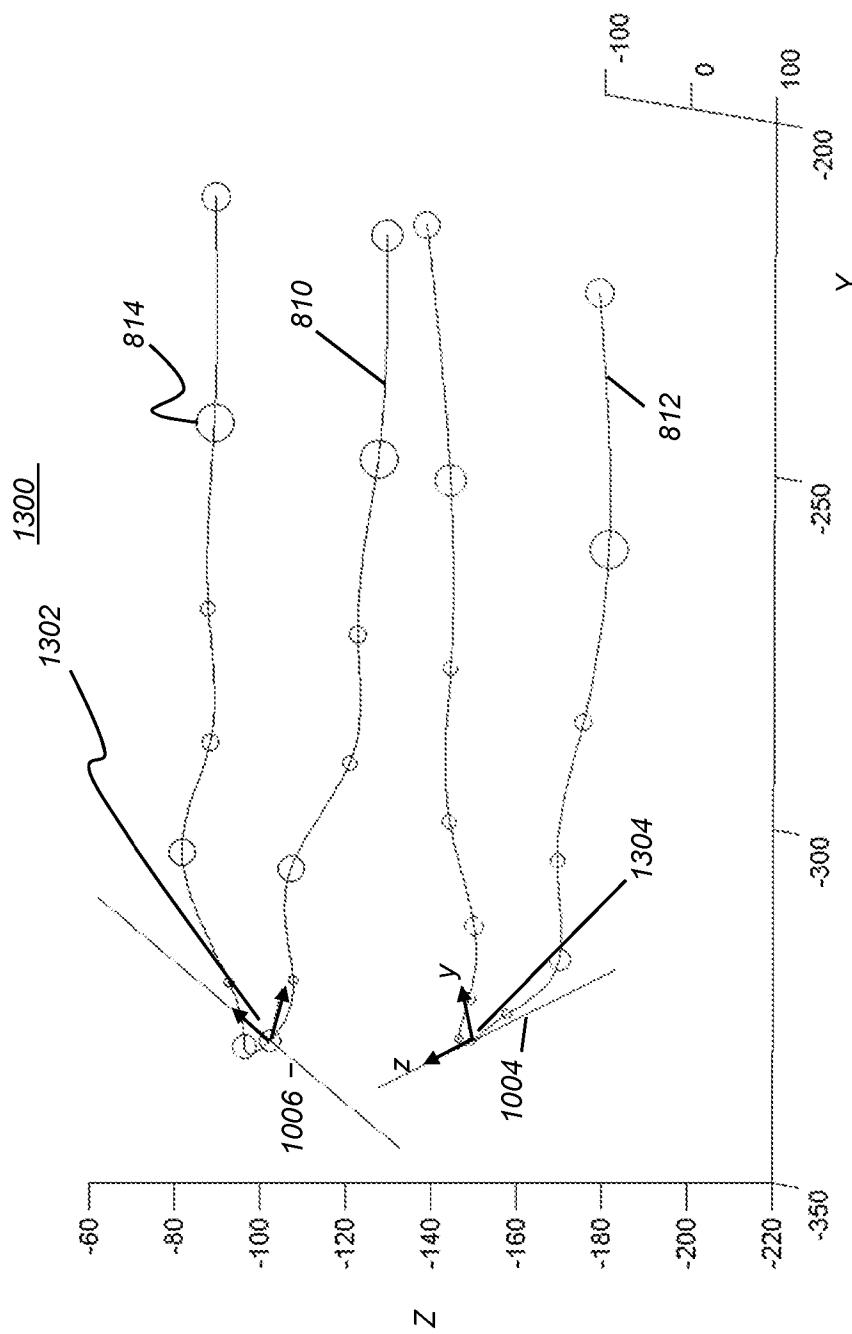


FIG. 13

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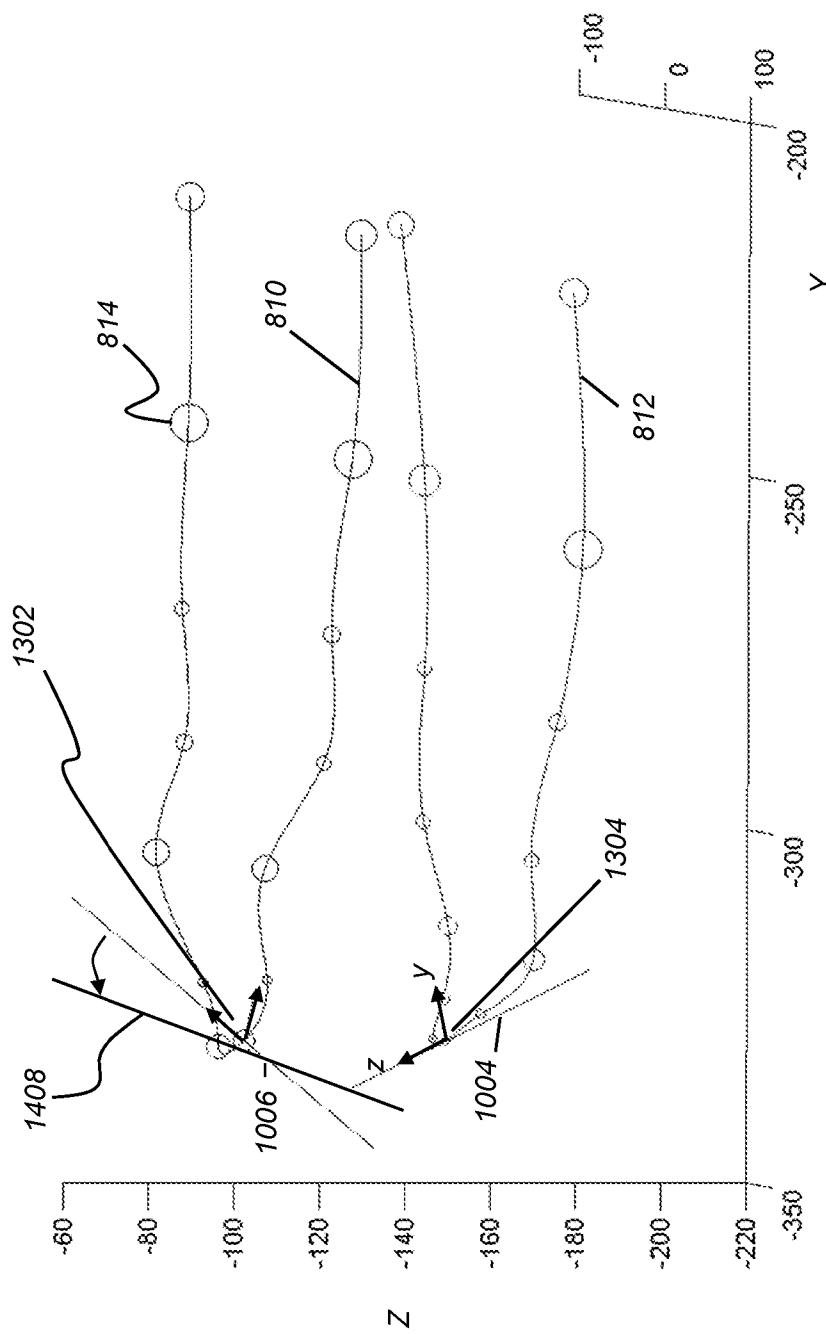


FIG. 14

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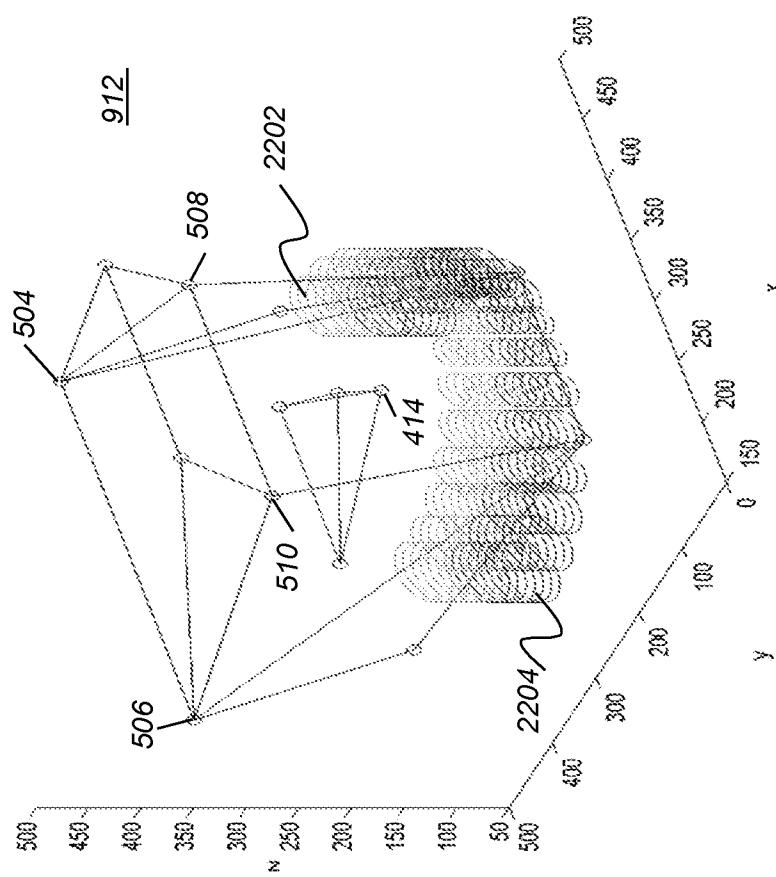


FIG. 15

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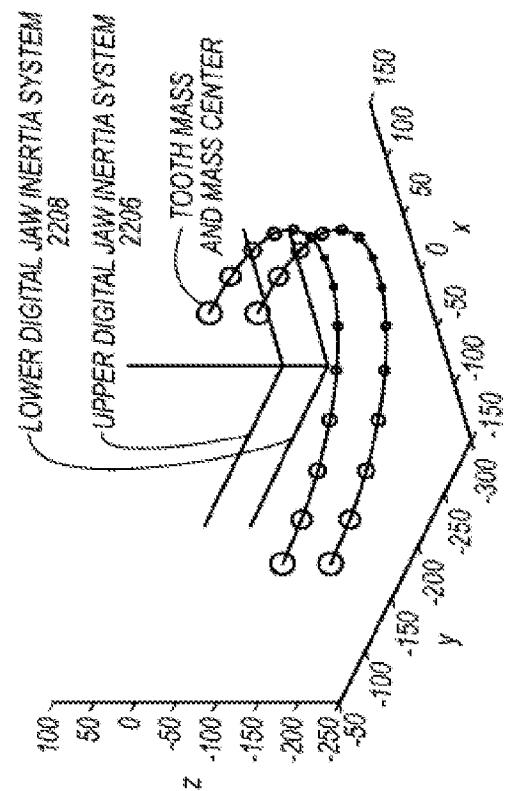


FIG. 16B

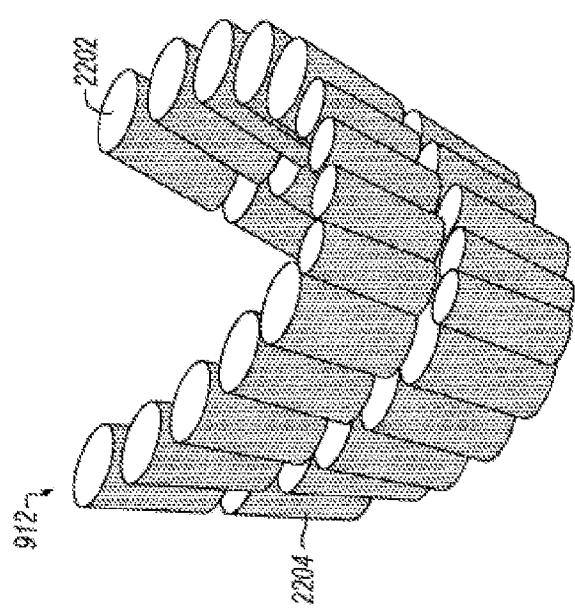


FIG. 16A

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FRONTAL VIEW

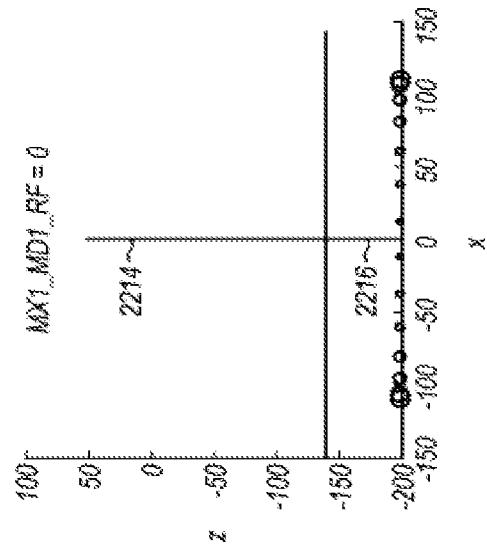


FIG. 17B

SAGITTAL VIEW

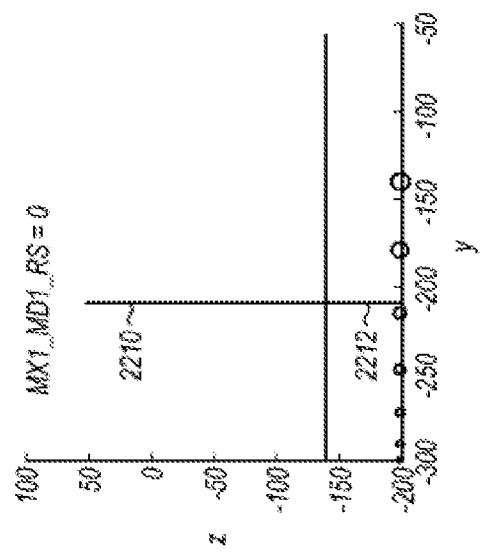


FIG. 17A

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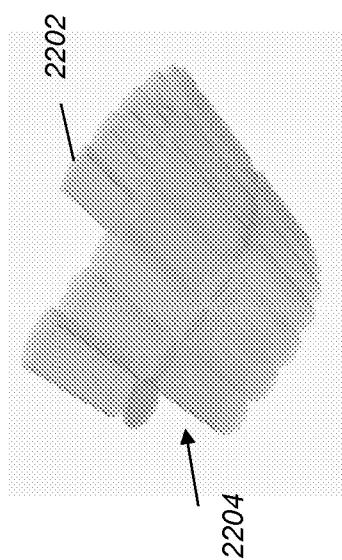
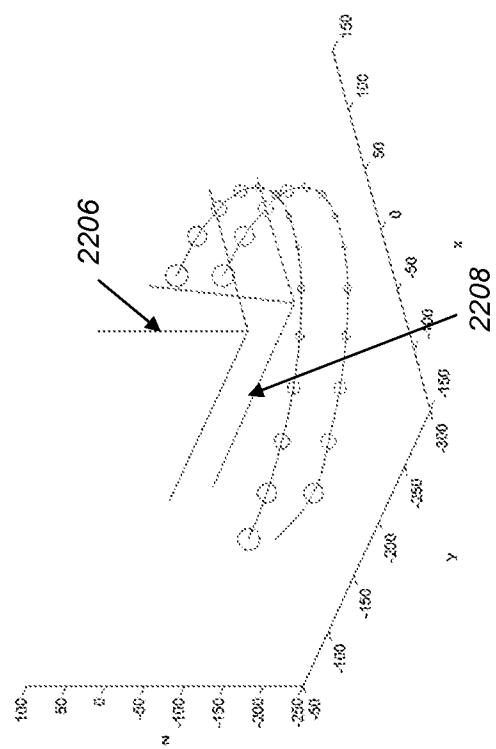


FIG. 18A

FIG. 18B

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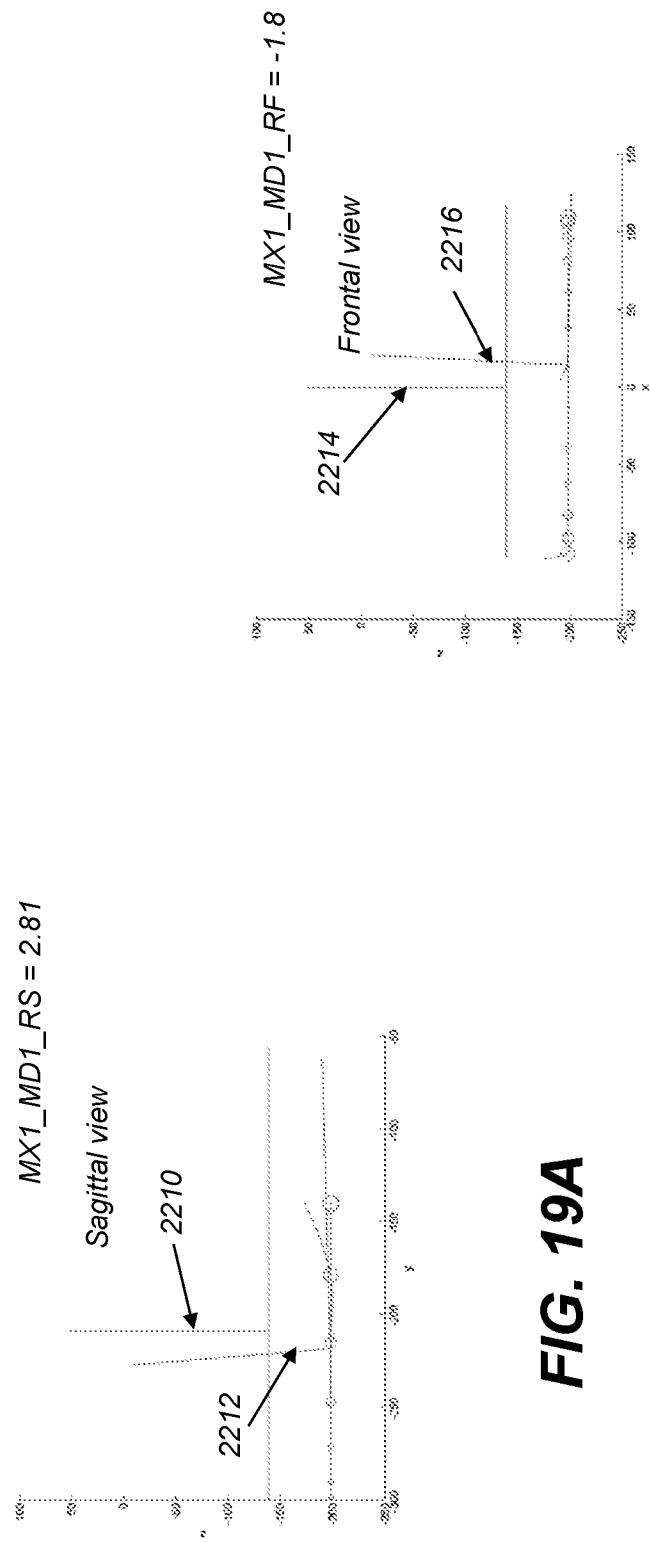


FIG. 19A

FIG. 19B

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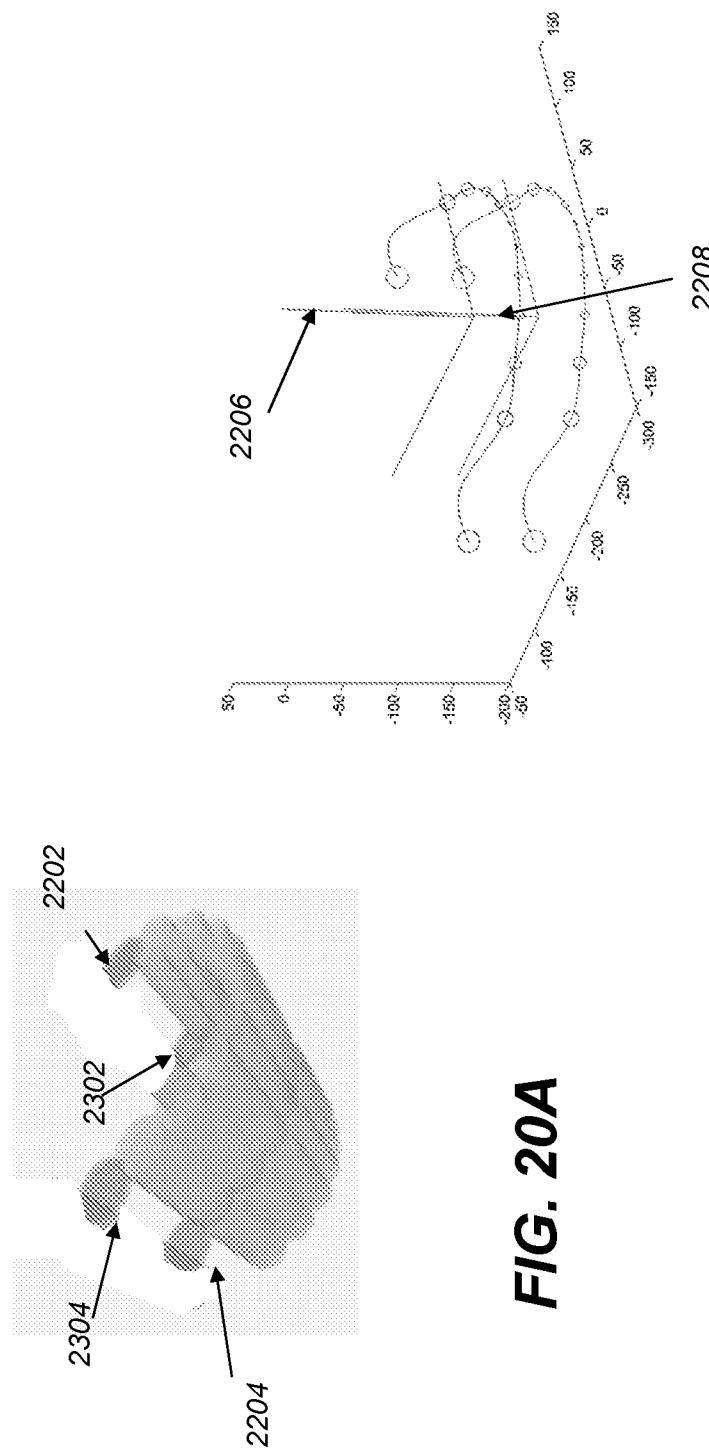
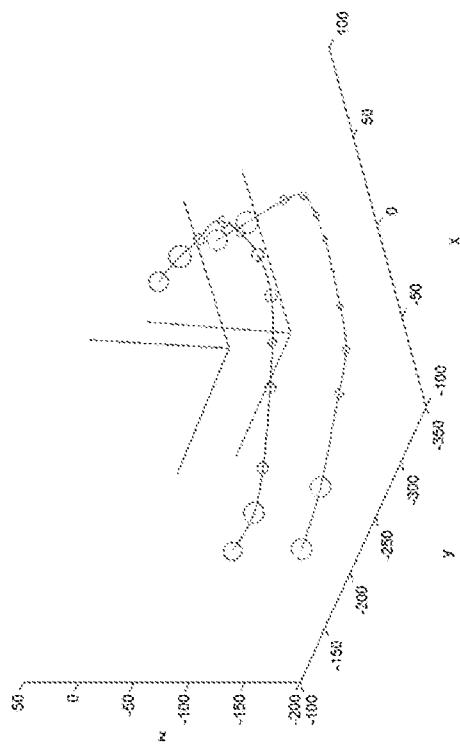
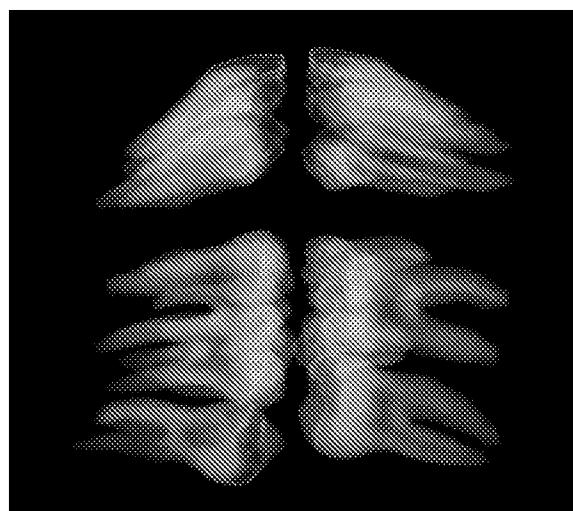


FIG. 20A

FIG. 20B

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Upper teeth &amp; lower teeth jaws principal inertia axes 3D view

2404**FIG. 21B**2402**FIG. 21A**

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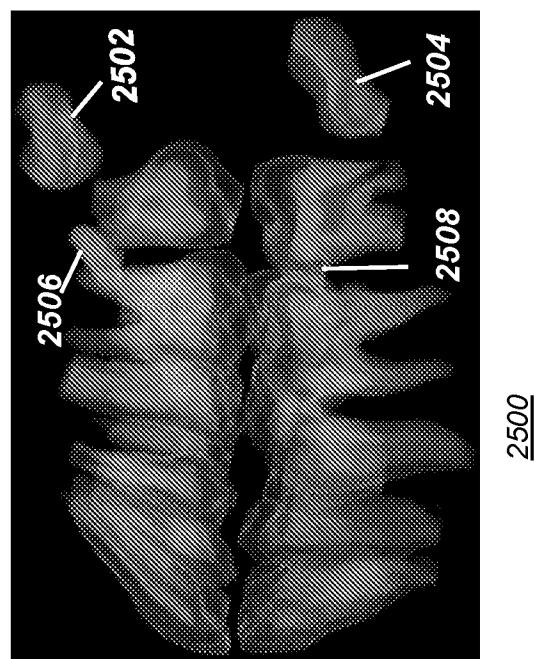
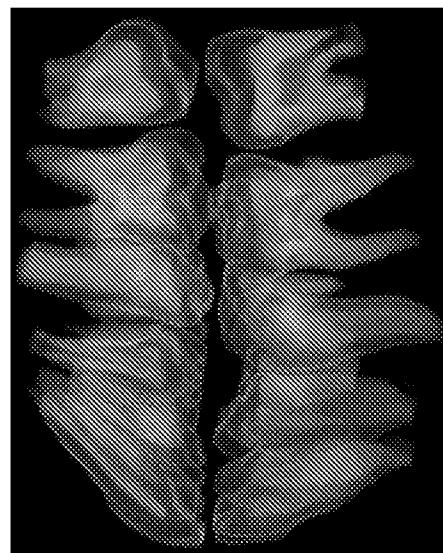
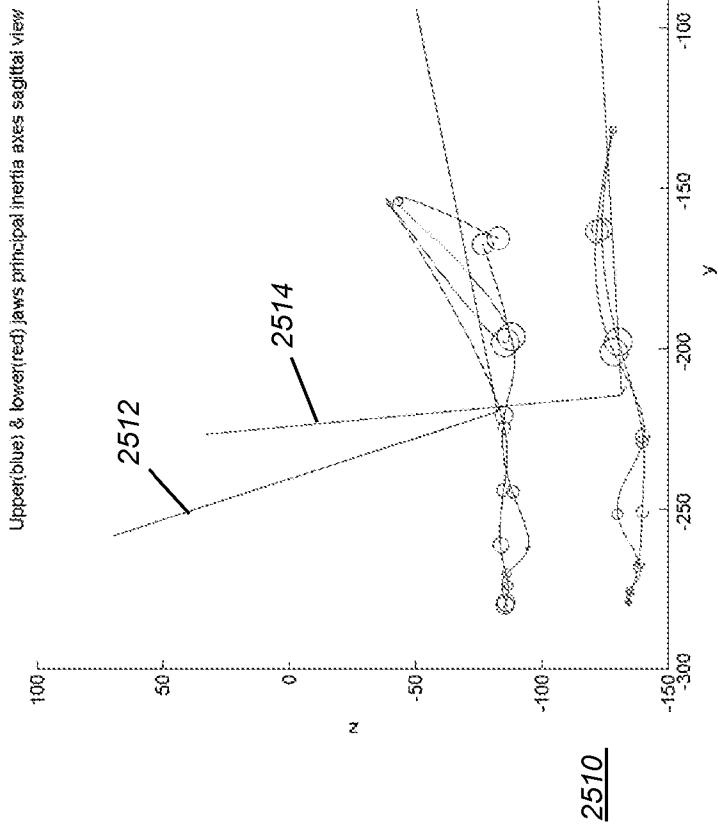


FIG. 22A

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2600**FIG. 23A****FIG. 22B**

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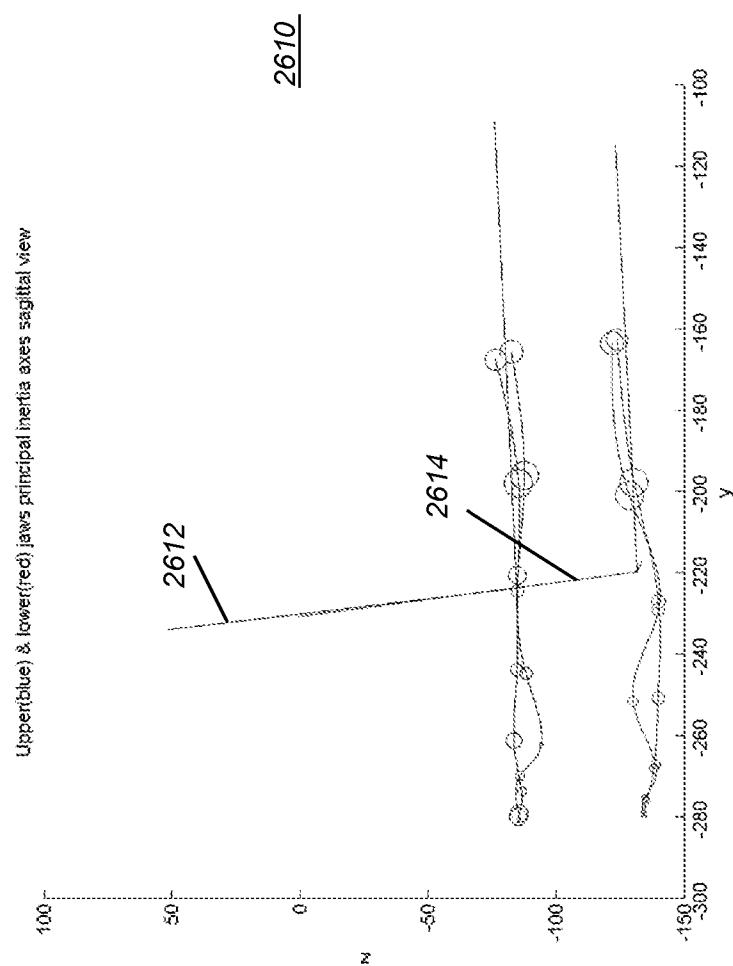


FIG. 23B

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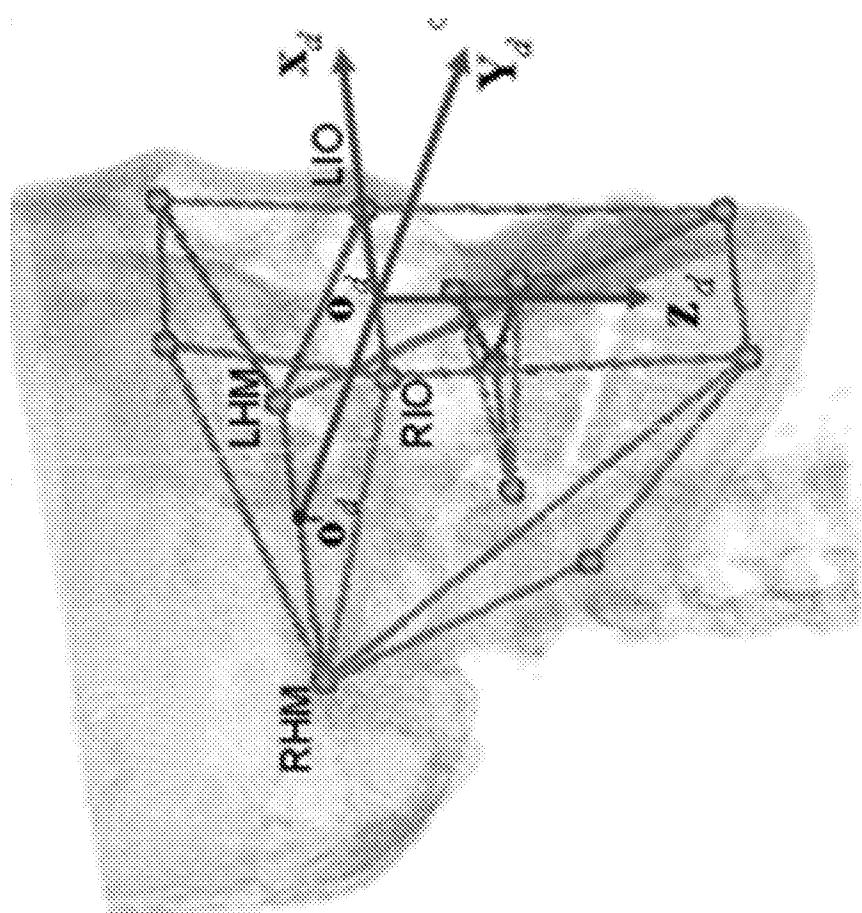
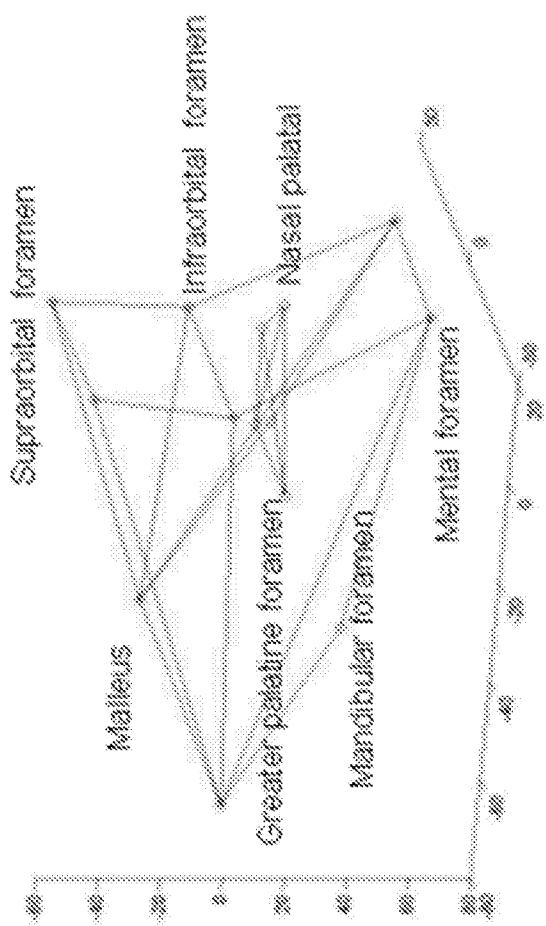
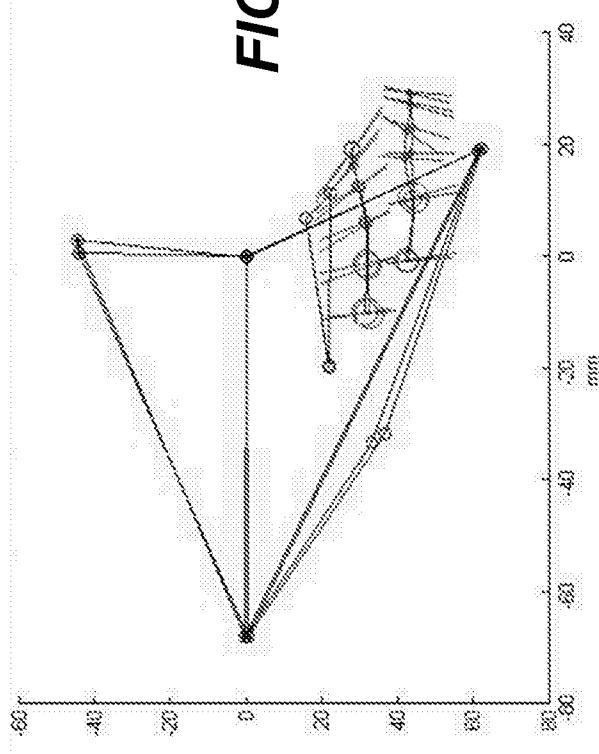


FIG. 24

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**FIG. 25****FIG. 26**

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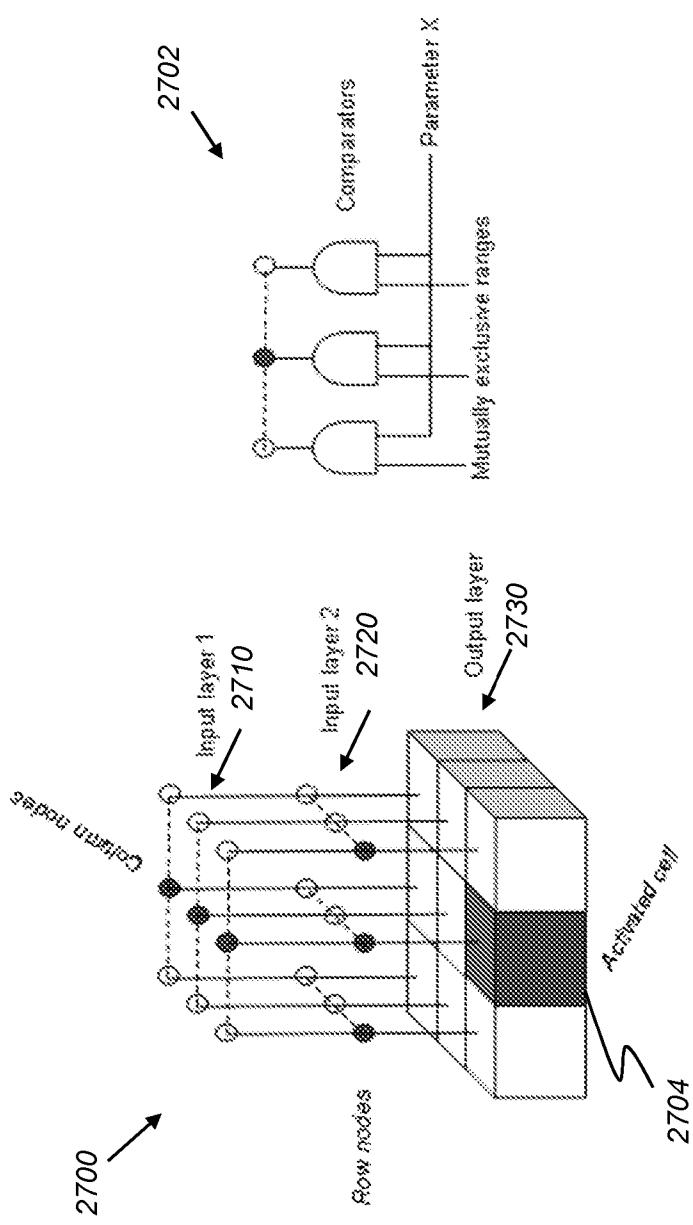


FIG. 27

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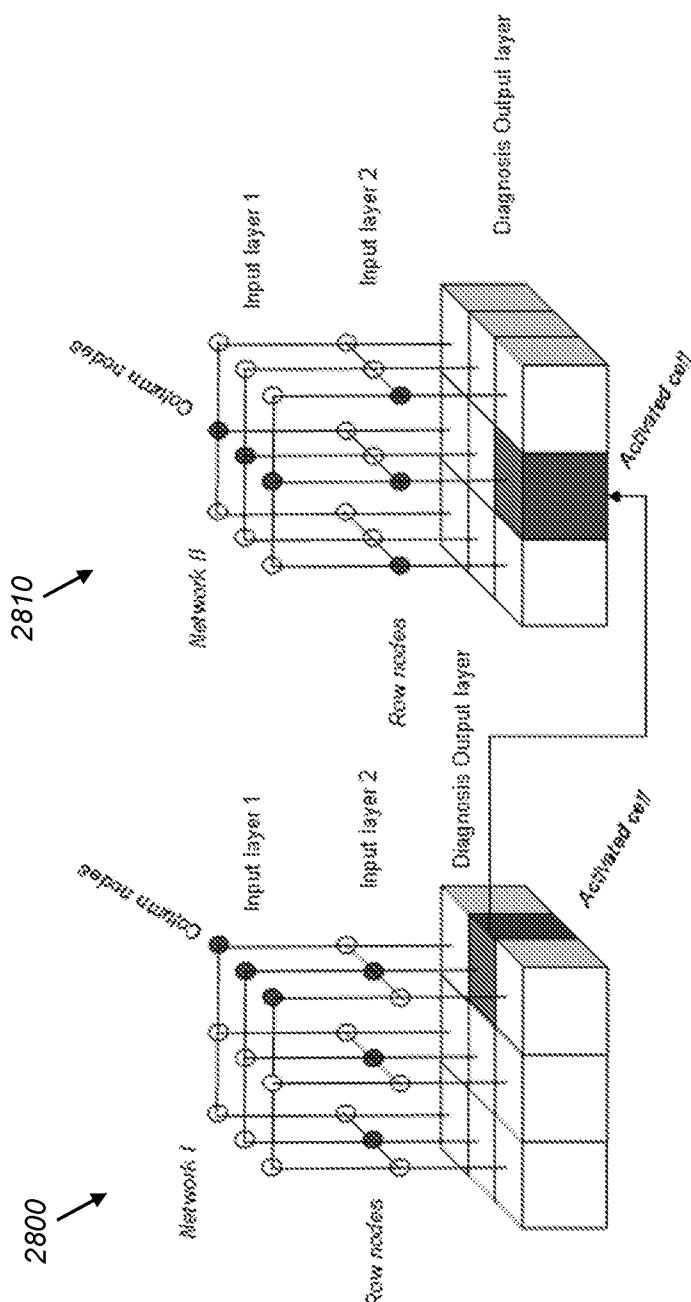


FIG. 28

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**FIG. 29**

independent\_diagnosis\_algorithm  
 $x_m, y_m \in [normal\_parameters, abnormal\_parameters]$   
 $x_m \neq y_m, m \in [1,2,\Lambda,13]$

given variables  $x_m, y_m$  :  
 define diagnosis\_result\_matrix(3x3)  $\mathbf{D}_m$   
 evaluate vector  $\mathbf{c}_m = [-\infty < x_m \leq \mu_{x_m} - \sigma_{x_m}, \mu_{x_m} - \sigma_{x_m} < x_m < \mu_{x_m} + \sigma_{x_m}, \mu_{x_m} + \sigma_{x_m} \leq x_m < \infty]$   
 evaluate vector  $\mathbf{r}_m = [-\infty < y_m \leq \mu_{y_m} - \sigma_{y_m}, \mu_{y_m} - \sigma_{y_m} < y_m < \mu_{y_m} + \sigma_{y_m}, \mu_{y_m} + \sigma_{y_m} \leq y_m < \infty]$   
 $\mu = Class\_I\_mean$  ;  $\sigma = Class\_I\_deviation$   
 $\mathbf{D}_m(i, j) = true$  if  $\mathbf{c}_m(j) = true$  and  $\mathbf{r}_m(i) = true$ ;  
 $i, j \in [1,2,3]$ .

dependent\_diagnosis\_algorithm  
 $x_k, y_k \in [normal\_parameters, abnormal\_parameters]$   
 $x_k \neq y_k, k \in [m, n], m, n \in [1,2,\Lambda,1,2,13], m \neq n$

**FIG. 30**

given variables  $x_k, y_k$  :  
 define diagnosis\_matrices(3x3)  $\mathbf{D}_m, \mathbf{D}_n$   
 evaluate vector  $\mathbf{c}_k = [-\infty < x_k \leq \mu_{x_k} - \sigma_{x_k}, \mu_{x_k} - \sigma_{x_k} < x_k < \mu_{x_k} + \sigma_{x_k}, \mu_{x_k} + \sigma_{x_k} \leq x_k < \infty]$   
 evaluate vector  $\mathbf{r}_k = [-\infty < y_k \leq \mu_{y_k} - \sigma_{y_k}, \mu_{y_k} - \sigma_{y_k} < y_k < \mu_{y_k} + \sigma_{y_k}, \mu_{y_k} + \sigma_{y_k} \leq y_k < \infty]$   
 $\mu = Class\_I\_mean$   $\sigma = Class\_I\_deviation$   
 $\mathbf{D}_m(i, j) = true$  if  $\mathbf{c}_m(j) = true$  and  $\mathbf{r}_m(i) = true$ ;  
 $\mathbf{D}_n(i, j) = true$  if  $\mathbf{c}_n(j) = true$  and  $\mathbf{r}_n(i) = true$ ;  
 $\mathbf{D}_m(i, j) = \mathbf{D}_m(i, j) + \mathbf{D}_n(i, j)$  if  $i + j \neq 4(exemplary)$   
 $i, j \in [1,2,3]; k \in [m, n]$ .

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1	Case Name: C1 III 9	
2	Eighteen Parameters	
3	Antero-posterior	
4	alveolar-GM-Gm	-10.479
5	alveolar-GM-Gm	-8.899
6	alveolar-Tgm	37.0168
7	alveolar-Tgm	11.2276
8	alveolar-GM+Gm/2 or Gv	2.3.0233
9	basis-MNP-MM	-10.0228
10	basis-MFM-MM	38.0601
11	architecture-MMV	19.0165
12	architecture-MHM-MM	106.922
13	Vertical	
14	alveolar-Gdz	37.0501
15	alveolar-MaxH-Mch	-6.8822
16	basis-<MaxH-Mch, MFM-MM>	27.609
17	architecture-MMz	61.97
18	architecture-13	33.4216
19	Transverse	
20	alveolar-CH-Mm	-0.4271
21	alveolar-Tgm-Tgm	27.5746
22	basis-RGP-LGP/RFM-LFM	36.2319
23	architecture-RD-LORM-MM	115.809
24	Deduced	
25	hidden-GM	17.7837
26	hidden-GM	28.2629
27	hidden-(Tgm+Tgm)/2	24.1472
28	hidden-(Tgm+Tgm)	25.7392
29	hidden-MNPv	6.98066
30	hidden-GM-MNPv	6.73502
31	hidden-GM-MMV	9.24639
32	hidden-3dz/MNPz-CHz	0.44501

FIG. 31A

ID	Measurement	Parameter	Current			Norm	mean	std	-5s	-4s	-3s	-2s	-1s	+3s	+4s	+5s
			min	dec	max											
1	Vertical		0.19		0.22	0.19	0.19	0.07	0.48	1.42	1.43	1.38	1.38	1.38	1.41	
2	2D arch. rot~Ghz-Ghz	0.1 Right/left lower molar height difference (+,Right lower) (T13)	0	-0.13	1.51	1.53	1.52	1.71	1.44							
3	2D arch. rot~Ghz-Ghz	0.32 Right/left lower molar height difference (+,Right lower) (T12)	0	0.15	1.22	1.22	1.22	1.22	1.21	1.21	1.21	1.21	1.21	1.21	1.21	
4	2D arch. rot~<RFL,Vx>	3.85 Mandible rolling (+,Right side lower) (T13)	0	-0.18	1.77	1.77	1.77	1.77	1.76	1.76	1.76	1.76	1.76	1.76	1.76	
5	2D arch. rot~<RFL,Vx>	0.51 Mandible rolling (+,Right side lower) (T12)	0	0.33	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	
6	2D arch. rot~arch. molar (Ghz-Ghz) (RFL-RFL)	-2.7 Right/left molar height difference (+,Right higher)	0	0.68	2.11	2.11	2.11	2.11	2.11	2.11	2.11	2.11	2.11	2.11	2.11	
7	2D bone rot~RFL-RFL	-0.32 Right/left molar height difference (+,Right lower)	0	0.44	1.23	1.23	1.23	1.23	1.22	1.22	1.22	1.22	1.22	1.22	1.22	
8	2D bone rot~RFL-RFL	2.8 Mandible right/left height difference (+,Right lower) (T14)	0	-0.82	2.98	2.98	2.98	2.98	2.98	2.98	2.98	2.98	2.98	2.98	2.98	
9	2D bone rot~RFL-RFL	1.44 Right/left molar height difference (+,Right higher)	0	0.44	2.06	2.06	2.06	2.06	2.06	2.06	2.06	2.06	2.06	2.06	2.06	
10	2D bone rot~<RFL-RFL,RFL-RFL>~UM-LHM-LHO>	-0.5 Difference of right/left basic mandible divergence	0	0.06	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	
11	2D bone rot~<RFL-RFL,RFL-RFL>~UM-LHM-LHO>	0.67 Difference of right/left basic mandible divergence	0	0.48	1.36	1.36	1.36	1.36	1.36	1.36	1.36	1.36	1.36	1.36	1.36	
12	2D arch. rot~<RFL,RFL,RFL>~<UM,LHM,LHO>	0.1 Difference of right/left global face divergences	0	0.08	1.78	1.78	1.78	1.78	1.78	1.78	1.78	1.78	1.78	1.78	1.78	
13	2D arch. rot~<RFL,RFL,RFL>~<UM,LHM,LHO>	-1.14 Right/left global face divergence	0	0.08	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	
14	2D arch. rot~<RFL,RFL,RFL>	0.53 Mandible right/left heights difference (T15)	0	-0.12	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	1.52	
15	2D arch. rot~<RFL,RFL,RFL>	-0.61 Right/left heights difference (T16)	0	0.06	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	1.22	

FIG. 31B

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Indx	Measure	Comment	Norm mean			
			std	$\pm S$	$\pm S$	$\pm S$
Anterior posterior						
1	AP_Gap~G25y-G36y	-0.11 1.18 1.25 1.16 1.16 1.16	0.206	1.22 1.22 1.22 1.22	1.29 1.29 1.29 1.29	1.30 1.30 1.30 1.30
2	alveolar_mis6ap~G46y-G36y	0.34 AP 46:36 difference (T16)	0	0.12 1.32 -1.2 1.44 -1.17	1.4	
3	AP_Gap~G25y-G36y	-0.51 0.51 0.51 0.51 0.51 0.51	0.197	1.40 1.86 1.43 1.81 1.81 1.81	1.81 1.81 1.81 1.81 1.81 1.81	1.81 1.81 1.81 1.81 1.81 1.81
4	alv_cmp_shifting~(G46-G36)y-(RFM-LFM)y	0.93 Lower molar AP position/manubrial right/left difference	0	-0.05 2.76 -2.31 2.21 -2.26	2.16	
5	AP_CU_R~G25y-G36y	1.5 1.5 1.5 1.5 1.5 1.5	0.189	1.38 1.89 1.83 1.83 1.83 1.83	1.53 1.53 1.53 1.53 1.53 1.53	1.53 1.53 1.53 1.53 1.53 1.53
6	alveolar_AP_CU_L~G26y-G36y	2 Left Class II; negative value means Class II relationship (T17)	-7.92	2.92 1.71 4.13 -1.71 -4.03	-1.67	
7	AP_Gap~G25y-G36y	-0.48 0.48 0.48 0.48 0.48 0.48	0.199	0.99 2.24 3.34 3.34 3.34 3.34	3.28 3.28 3.28 3.28 3.28 3.28	3.28 3.28 3.28 3.28 3.28 3.28
8	bass_morpho~RGPy-LGPy	0.38 AP great palatal right/left position difference (T18)	0	0.32 1.34 -1.02 1.66 -0.99	1.62	
9	AP_Gap~G25y-G36y	-0.59 0.59 0.59 0.59 0.59 0.59	0.197	1.27 1.86 1.83 1.83 1.83 1.83	1.66 1.66 1.66 1.66 1.66 1.66	1.66 1.66 1.66 1.66 1.66 1.66
10	arch_AP_RL_FcExss~(RIO-RHM)-(LIO-LHM)	-0.33 Facial depth right/left difference (FDO level)	0	-0.09 2.95 -3.05 2.86 2.98 2.79		
11	AP_Gap~G25y-G36y	0.72 0.72 0.72 0.72 0.72 0.72	0.222	1.22 1.22 1.22 1.22 1.22 1.22	1.56 1.56 1.56 1.56 1.56 1.56	1.56 1.56 1.56 1.56 1.56 1.56
12	arch_AP_RL_FcExss~RSDy-LSDy	0.55 AP SPO positions, right/left difference	0	0.31 1.46 -1.15 1.77 -1.12	1.73	
13	AP_Gap~G25y-G36y	-1.07 AP dental positions, right/left difference (T19)	0	0.88 1.12 1.26 0.88 1.28 1.28	1.28 1.28 1.28 1.28 1.28 1.28	1.28 1.28 1.28 1.28 1.28 1.28
14	arch_AP_RL_FcExss~(RM-RHM)-(L4-LHM)	-1.4 Facial depth right/left difference (mental level) projected on Y	0	-0.85 2.63 -3.48 1.78 -3.39	1.74	
15	AP_Gap~G25y-G36y	-1.29 1.29 1.29 1.29 1.29 1.29	0.222	1.06 1.46 1.47 1.36 1.47 1.47	1.38 1.38 1.38 1.38 1.38 1.38	1.38 1.38 1.38 1.38 1.38 1.38
16	addition_AP_RL~(G16y-G46y)-(G25y-G36y)	-0.45 Class 2 right/left difference	0	0.17 0.81 0.98 0.64 0.95 0.63		

FIG. 31C

SUBSTITUTE SHEET

SUBSTITUTE SHEET (RULE 26)

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Index	Measure	Comment	Norm	mean	std	-S	+S	-SS	+SS
1	av.gr.bor.transv.pos~Gnx	0.14 Lower incisor transverse deviation (14)	0.612	1.26	1.3	1.65	1.3	1.3	1.3
2	av.gr.bor.transv.pos~Gnx	0.19 Lower incisor transversal deviation (15)	0	-0.1	2.09	-2.2	1.99	-2.1	1.94
3	av.gr.bor.transv.pos~Gnx	0.97 Lower incisor transversal deviation	0.838	1.3	1.3	1.78	1.3	1.3	1.3
4	av.gr.bor.transv.pos~Gnx	0.58 Lower arch transversal deviation	0	-0.1	1.89	-2	1.8	-1.9	1.76
5	av.gr.bor.transv.pos~Gnx	0.04 Lower arch transversal deviation (16)	0.694	1.3	1.3	1.54	1.3	1.3	1.3
6	av.gr.bor.transv.pos~Gnx	0.51 Lower molar transversal deviation (17)	0	0.01	1.92	-1.9	1.92	-1.9	1.88
7	av.gr.bor.transv.pos~Gnx	-0.91 Lower molar transversal deviation (18)	0.632	1.3	1.3	2.3	1.3	1.3	1.3
8	av.arch.ratn.<Mfl.Wy>(RH)	1.31 Lower arch rotation in arch plane (+:Right) (13)	0	-0	2.8	-2.8	2.78	-2.8	2.78
9	av.bn.transv.comp~Gnx.Mx	-0.22 Deviation: upper incisor-mandible anterior landmark	0.643	1.3	1.3	1.53	1.3	1.3	1.3
10	av.bn.transv.comp~Gnx.Mx	-0.35 Deviation: lower incisor-mandible anterior landmark	0	0.41	0.59	-0.3	1.09	-0.3	1.07
11	av.bn.transv.comp~Gnx.Mx	1.12 Deviation: upper molar-mandible anterior landmark	0.606	1.3	1.3	1.52	1.3	1.3	1.3
12	av.bn.transv.comp~Gnx.GBnx	0.17 Deviation: lower arch-mandible	0	0.26	0.79	-0.5	1.05	-0.5	1.03
13	av.bn.transv.comp~Gnx.GBnx	0.62 Deviation: upper molar-mandible anterior landmark	0	0.31	0.74	-0.5	1.05	-0.5	1.03
14	av.bn.transv.comp~Gnx.MFx	0.47 Deviation: lower molar-posterior mandible	0	0.18	1.16	-1	1.34	-1	1.31
15	av.bn.transv.comp~Gnx.Mx	-1.11 Upper arch rotation in arch plane (+:Left) (19)	0	1.32	2.4	-1.1	2.22	-1.1	2.22
16	av.bn.tor.comp~TQ_37_TQ_46_4	1.24 Upper molar torque compensation of mandible right deviation	0	-1.5	4.18	-5.8	2.58	-5.8	2.58
17	av.bn.tor.comp~TQ_37_TQ_46_4	-0.12 Upper molar torque compensation of mandible left deviation (19)	0	0.32	1.12	-0.7	1.31	-0.7	1.31
18	av.bn.tor.dev~Gnx.Gnx	0.4 Upper/lower arch left deviation	0	0.27	0.98	-0.6	1.14	-0.6	1.12
19	av.bn.tor.dev~Gnx.Gnx	-0.5 Upper/lower arch right deviation (19)	0	0.94	2.8	-0.7	3.8	-0.7	3.8
20	av.bn.adult.dev~<Mfl.Wy>	3. Upper/lower arch right deviation (+: maxilla right deviation) (12)	0	0.6	2.53	-1.9	3.13	-1.9	3.13
21	base.bone.U1.bn.dev~MFx	-0.6 mid-mandible-foramen left deviation	0	0.24	2.26	-1.4	2.26	-1.4	2.26
22	base.bone.U1.bn.dev~MFx	0.04 mid-mandible-foramen left deviation	0	-0.2	2.05	-2.2	1.87	-2.2	1.83
23	base.bone.U1.bn.dev~MFx	0.34 mid-mandible-foramen left deviation (13)	0	0.32	1.8	-0.8	1.42	-0.8	1.42
24	base.bone.U1.bn.dev~MFx	0.76 mid-mandible-foramen left deviation (10)	0	-0.5	2.23	-2.7	1.72	-2.7	1.68
25	base.bone.U1.bn.dev~MFx	-0.1 mid-mandible-foramen left deviation (10)	0	0.23	1.9	-1	1.22	-1	1.22
26	base.bone.U1.bn.dev~Gnx	0.4 Mandible left deviation	0	-0.3	1.96	-2.3	1.62	-2.3	1.58
27	base.bone.U1.bn.dev~Gnx	-0.6 Mandible left deviation (19)	0	0.21	2.2	-1	1.31	-1	1.31
28	base.bone.U1.bn.dev~MNPx-MFx	-0.4 Maxilla-mandible anterior left deviation (18,T9,T10,T11)	0	0.83	1.52	-0.7	2.35	-0.7	2.3
29	base.bone.U1.bn.dev~Gnx.Gnx	-0.5 Maxilla-mandible anterior left deviation (18)	0	0.37	1.18	-0.7	1.65	-0.7	1.65
30	arch facial devn~NSOx.MFx	-3.2 Chin facial deviation	0	0.67	3.1	-2.4	3.77	-2.4	3.68
31	arch facial devn~NSOx.MFx	-0.82 Chin facial deviation	0	-0.24	4.2	-2.3	3.32	-2.3	3.32
32	arch facial devn~2_angle	90.5 Oral/face bearing left deviation	0	0.82	1.82	0.8	2.16	0.8	2.16

FIG. 31D

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A	B	C	D
Indics relation [1] of vs Arches angle relation [2] row	Under net upper/lower incisors negative gap [1]	Overt upper/lower incisors positive gap [4]	Overt upper/lower incisors positive gap [4]
Occlusal Class III upper/lower arches relation [1]	Underjet with Class III	Class III desirous incisors relation	Overt and contradictory Class II
Occlusal Class I upper/lower arches relation	Underjet without Class III	...	Overt without Class II
Occlusal Class II upper/lower arches relation [1]	Underjet and contradictory Class II	...	Overt with Class II
AI 1 Matching incisors and global arches arches positive upper/lower discrepancy	Class II desirous incisors relation	...	...
Case Name: Cf III 9			

FIG. 32A

A	B	C	D
Indics relation [1] of vs Arches angle relation [2] row	Under net upper/lower incisors negative gap [1]	Overt upper/lower incisors positive gap [4]	Overt upper/lower incisors positive gap [4]
Occlusal Class III upper/lower arches relation [1]	Underjet with Class III	Class III desirous incisors relation	Overt and contradictory Class II
Occlusal Class I upper/lower arches relation	Underjet without Class III	...	Overt without Class II
Occlusal Class II upper/lower arches relation [1]	Underjet and contradictory Class II	Class II desirous incisors relation	Overt with Class II
AI 1 Matching incisors and global arches arches positive upper/lower discrepancy	...	...	...
Case Name: Cf III 9			

FIG. 32B

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3200	3200	3200	3200
Gy (z) vs Global moments torque (21) row	Linear bifurcation (-)	0	Linear bifurcation (+)
Angular bifurcation (-)	Linear and angular bifurcation	Angular bifurcation	Linear bifurcation despite angular bifurcation
0	Linear bifurcation	Linear bifurcation	Linear bifurcation
Angular bifurcation (+)	Linear bifurcation despite angular bifurcation	Angular bifurcation	Linear and angular bifurcation
All Linear and angular bifurcation	Linear bifurcation	Angular bifurcation	Linear bifurcation

CASE NAME: 9500 9500 VOL 16

FIG. 32C

3292		Column 0	Column 1	Column 2	Column 3
Row 0	Incisors transverse relation TNS17c (GIMx-Ginx) vs molars transverse relations TNS19 r (GIMx-Ginx)	Upper/Lower incisors right deviation (-)	0	Upper/Lower incisors left deviation (+)	
Row 1	Upper/Lower molars transverse right deviation (-)	Global upper arch right translation/lower	Posterior upper/lower arch right deviation	Upper arch left global rotation/lower	
Row 2	0	Upper/Lower incisors right deviation	0	Upper/Lower incisors left deviation	
Row 3	Upper/Lower molars transverse left deviation (+)	Upper/arch right global rotation lower	Posterior upper/lower arch left deviation	Global upper arch left translation/lower	

FIG. 32E

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CASE NAME: 9500 9500 VOL 16

Af	PARAMETERS	DIAGNOSIS
Af 1	Matching incisors and global arches anterior position upper/lower	incisors relation (11;128 vs Anterior angle relation 0°) row
Af 2	Matching incisors discrepancy and separate mean upper/lower incisors positions	incisors relation (11;128 vs Upper incisor position 19°) row
Af 3	Matching incisors discrepancy and separate mean upper and lower incisors positions	incisors relation (11;128 vs Lower incisor position 20°) row
Af 4	Matching incisors gap & upper/lower CL II torque differential (CL II compensation)	incisors relation (11;128 vs Torque Upper/lower difference 0°) row
Af 5	Upper/lower separate responsibilities concerning upper/lower CL II torque differential (CL II compensation)	Upper incisors torque (33; 34) vs Lower incisors torque (31; 32) row
Af 6	Matching adiector and basic upper/lower relationship	Dental Class II (21; 22) vs basic Class II (31; 32) row
Af 7	Upper/lower separate responsibilities concerning skeletal CL II and CL III	MPF (23; 24) vs MPF (31; 32) row
Af 8	Linear and angular skeletal/soft tissue relationship	Gy (33; 34) vs Facial incisors torque (21; 22) row
Af 9	Global linear facial vertical height and its distribution	WHA (10; 108) vs GFM (11; 108)
Af 10	Linear and angular facial distribution	WHA (10; 108) vs 13 (14) row
Af 11	Anterior and basic divergences	Ant. Molar (11) (23) vs FMA (12; 13) row
Af 12	Transverse linear and angular upper/lower anterior relationship	WHA (15; 109) vs TMA-Tan (16; 109) row
Af 13	Transverse linear and angular upper/lower basic relationship	RGP-LSP-FM-LM (17; 109) vs ROL-LSP-LM (18; 109) row

**FIG. 32D**

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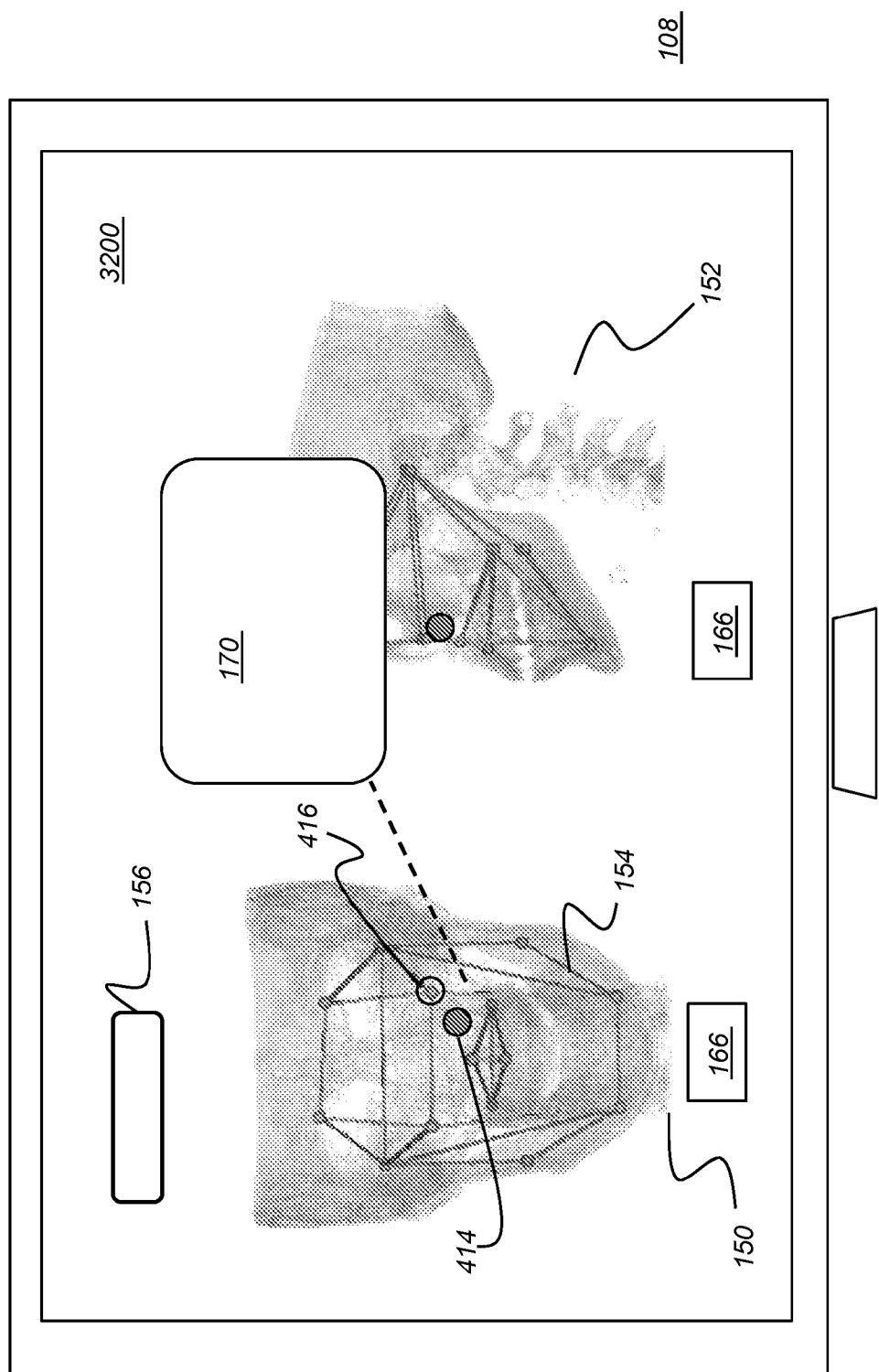


FIG. 33

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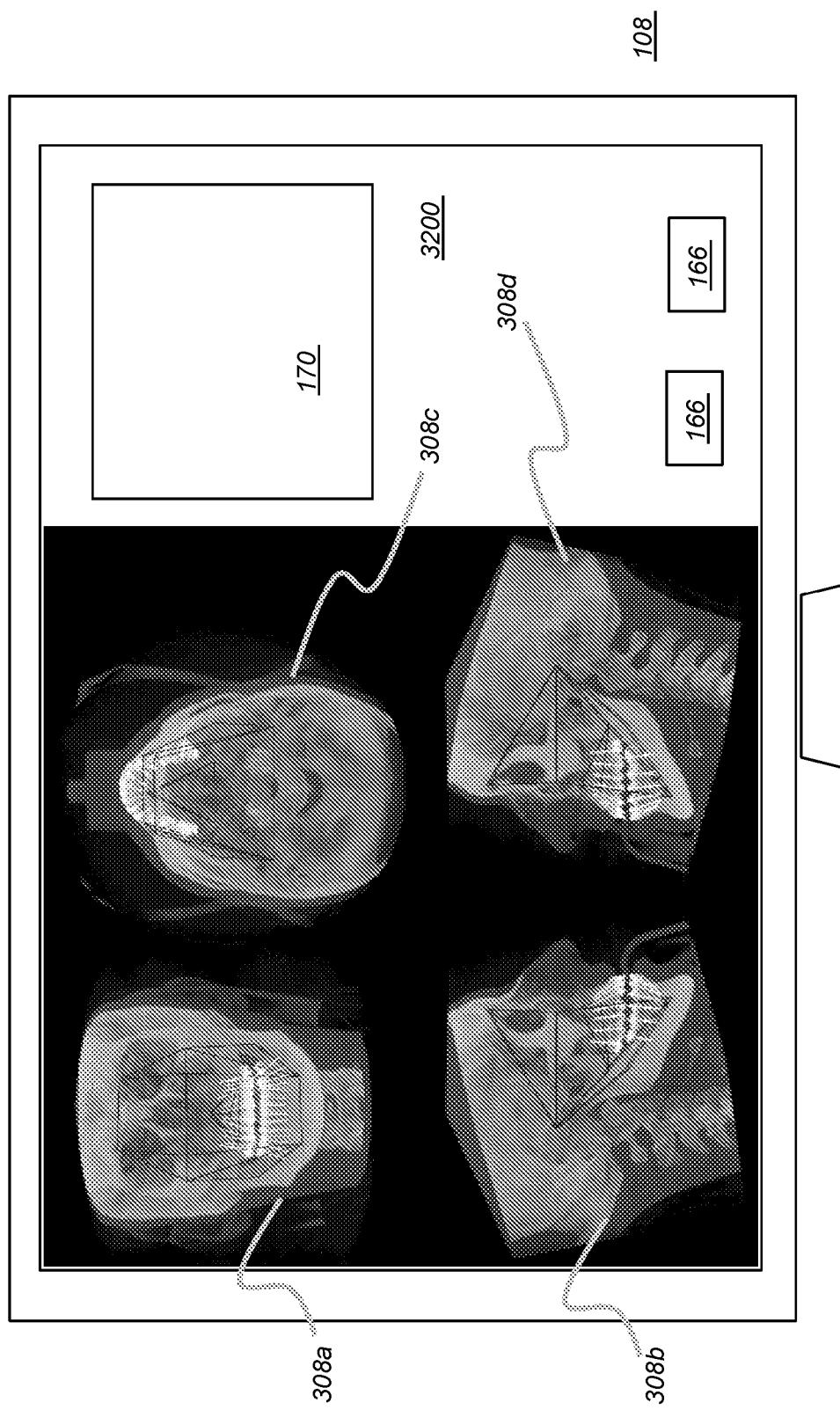


FIG. 34

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T1; P19,17;C2,1; Upper/Lower incisors right deviation

T2; P20;C1,2; 0

T3; P8,7;C2,2; 0

T4; P1,17;C2,1; Upper/lower incisors right deviation

T5; P2,17;C2,1; 0

T6; P5,19;C2,2; 0

T7; P6,19;C2,2; 0

T8; P27,28;C2,1; 0

T9; P23,28;C2,1; 0

T10; P24,28;C3,1; Upper/Lower anterior landmarks right deviation is due to chin left deviation

T11; P28,17;C1,1; The upper/Lower incisors right deviation is in agreement with upper/lower base dev

T12; P3,1;C2,2; --

T13; P4,2;C2,2; --

T14; P8,7;C2,2; --

T15; P15,14;C2,2; 0

T16; P2,1;C2,2; 0

T17; P6,5;C3,2; Left Class II

T18; P9,8;C2,2; --

T19; P13,7;C3,3; Excess of the right hemiface and of the right horizontal branch

S1 Anterior-posterior direction synthetic comment = strong right anteroposterior excess

S2 Vertical direction synthetic comment = none

S3 Transversal direction synthetic comment = left upper deviation (right excess ) tendency

**FIG. 35**

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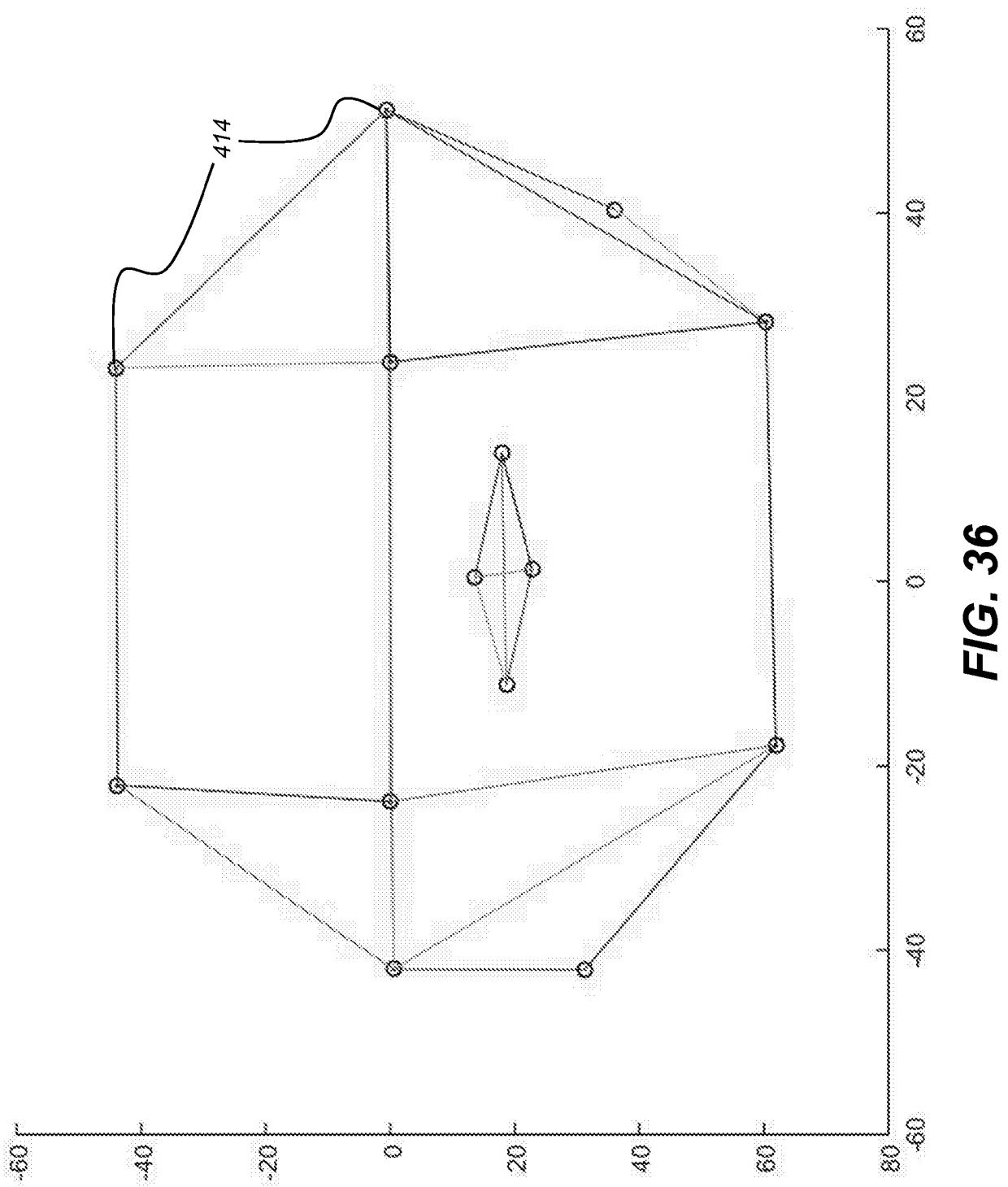


FIG. 36

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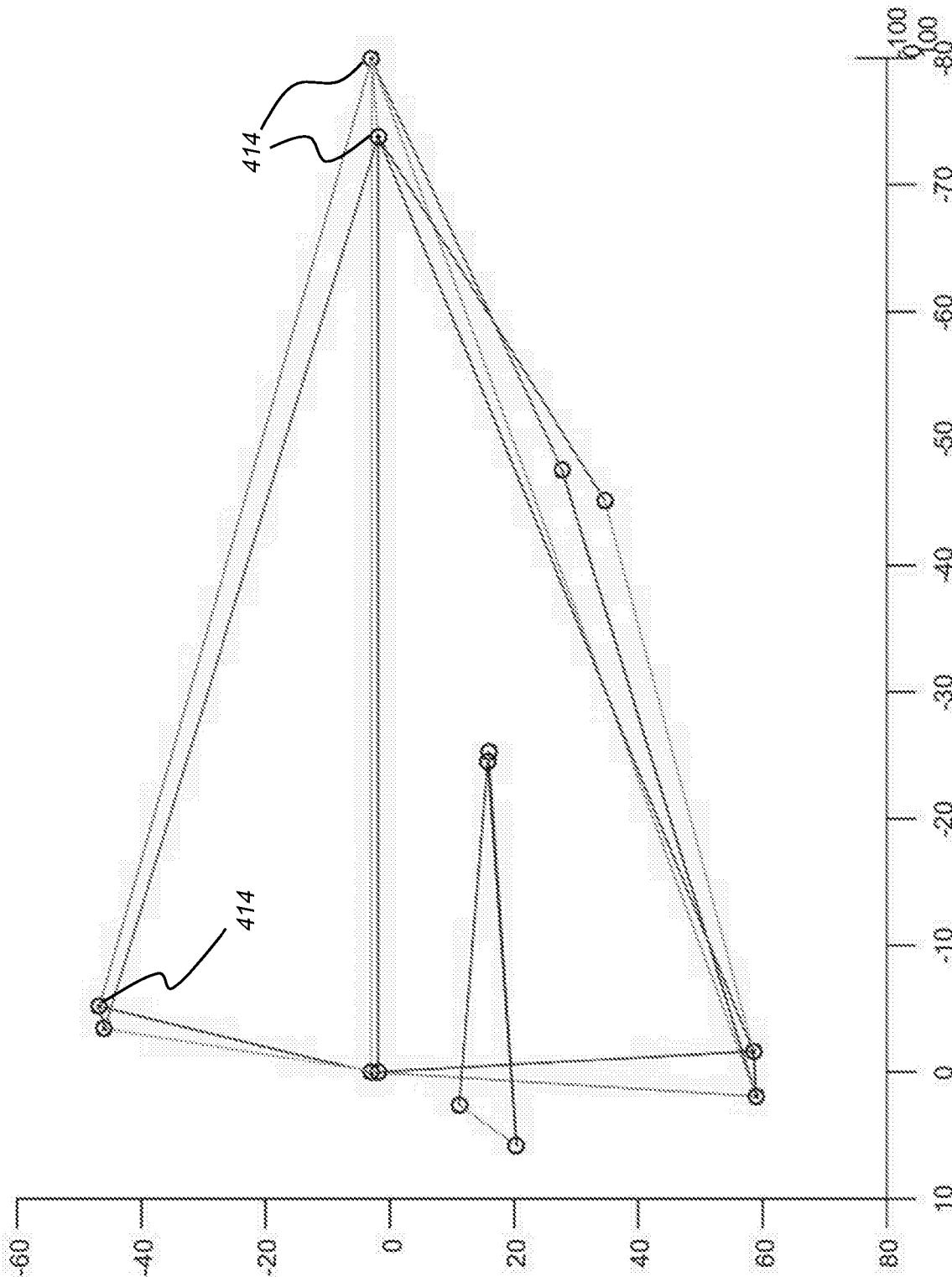


FIG. 37

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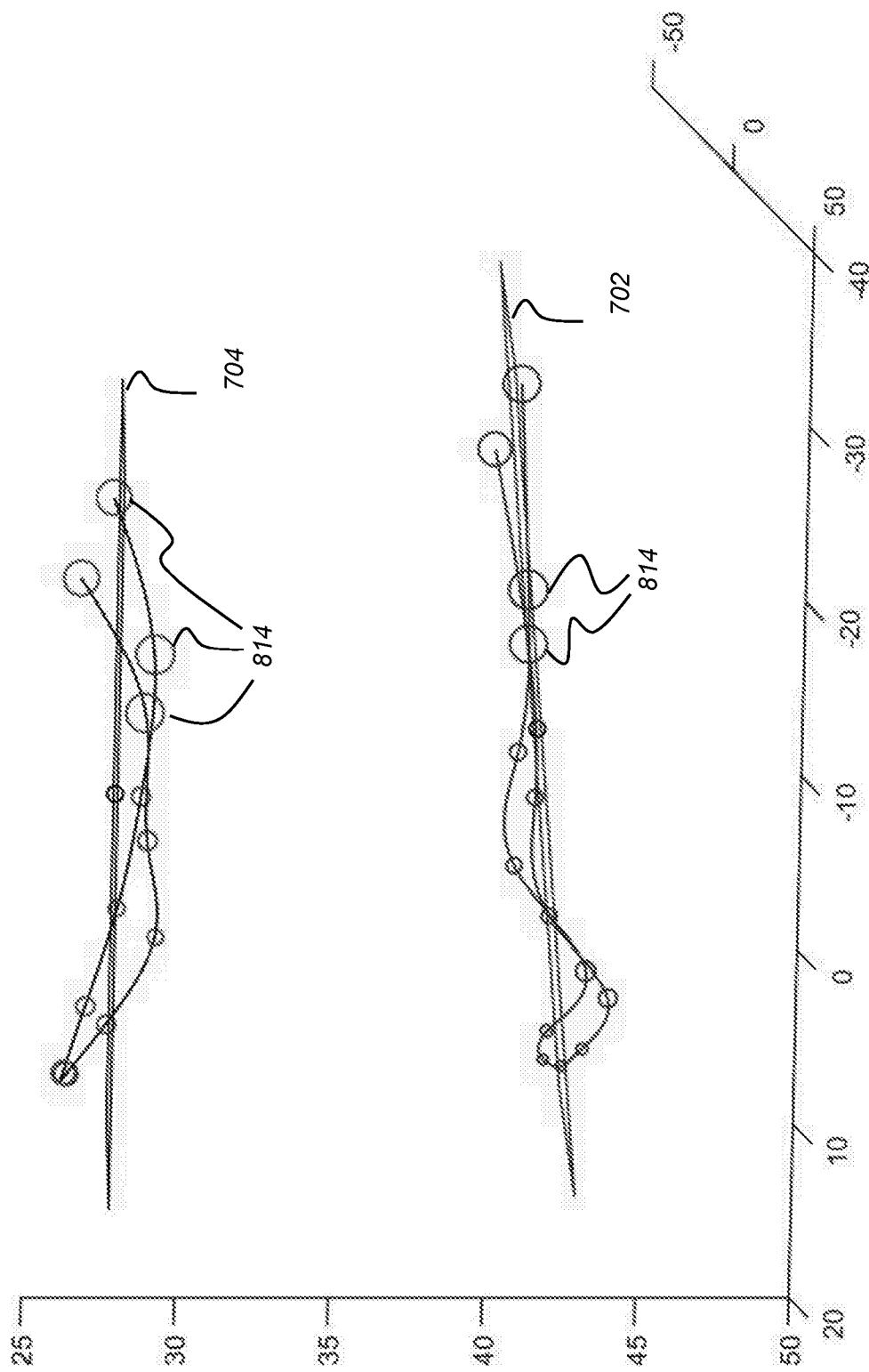


FIG. 38

# INTERNATIONAL SEARCH REPORT

International application No  
PCT/GB2017/053885

**A. CLASSIFICATION OF SUBJECT MATTER**  
INV. G06T7/00  
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)  
G06T A61B G06K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-Internal, INSPEC, WPI Data

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2014/348405 A1 (CHEN SHOUPU [US] ET AL) 27 November 2014 (2014-11-27) abstract figures 2,5,6,9,10 paragraphs [0011], [0062], [0067], [0073], [0077], [0089], [0127] -----	1-12
A	US 8 805 048 B2 (BATESOLE MARK [US]) 12 August 2014 (2014-08-12) abstract figure 2 column 4, line 4 - line 24 column 5, line 46 - line 61 column 6, line 49 - line 60 column 1, line 24 ----- -/-	1-12

Further documents are listed in the continuation of Box C.

See patent family annex.

\* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
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"&" document member of the same patent family

Date of the actual completion of the international search	Date of mailing of the international search report
15 March 2018	26/03/2018

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Fax: (+31-70) 340-3046

Authorized officer

Scholz, Volker

## INTERNATIONAL SEARCH REPORT

International application No
PCT/GB2017/053885

## C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	<p>MARI ELI LEONELLI DE MORAES ET AL:          "Evaluating craniofacial asymmetry with digital cephalometric images and cone-beam computed tomography",          AMERICAN JOURNAL OF ORTHODONTICS AND DENTOFACIAL ORTHOPEDICS,          vol. 139, no. 6,          1 January 2011 (2011-01-01), pages e523-e531, XP028224044,          ISSN: 0889-5406, DOI:          10.1016/J.AJODO.2010.10.020          [retrieved on 2011-03-14]          abstract          figures 1-3          tables I,II</p> <p>-----</p> <p>KANG YOUNG CHOI: "Analysis of Facial Asymmetry",          ARCHIVES OF CRANIOFACIAL SURGERY,          vol. 16, no. 1,          1 January 2015 (2015-01-01), page 1,          XP055455931,          ISSN: 2287-1152, DOI:          10.7181/acfs.2015.16.1.1          abstract          figure 7          tables 4,5</p> <p>-----</p> <p>J. Treil ET AL: "The Human Face as a 3D Model for Cephalometric Analysis",          CGS Volume 43: Digital Radiography and Three-Dimensional Imaging,          1 January 2015 (2015-01-01), XP055455545,          Retrieved from the Internet:          URL:<a href="https://orthodonticbooks.com/product/cgs-volume-43-digital-radiography-and-three-dimensional-imaging/">https://orthodonticbooks.com/product/cgs-volume-43-digital-radiography-and-three-dimensional-imaging/</a>          [retrieved on 2018-03-01]          cited in the application          page 143</p> <p>-----</p>	1-12
A		1-12
A		1-12

**INTERNATIONAL SEARCH REPORT**

Information on patent family members

International application No  
PCT/GB2017/053885

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			WO 2015009589 A1 22-01-2015
US 8805048	B2	12-08-2014	NONE