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(54) **Title:**
**DUAL FEEDBACK VACUUM FLUIDICS FOR A FLOW-TYPE
PARTICLE ANALYZER**

(57) **Abstract:**

The present invention relates to a vacuum-driven fluidic system for a flow-type particle analyzer. The system includes a vacuum pump which creates a pressure drop downstream of the flow cell, which pulls sheath fluid and sample fluid through the flow cell. A variable-resistance fluidic resistor is configured to control the ratio of sample fluid flow to sheath fluid flow. Dual feedback circuits, one configured to modulate the vacuum pump power in response to the pressure drop across the flow cell, referred to as the dynamic pressure drop, and a second configured to modulate the vacuum pump power in response to the pressure drop created by the vacuum pump relative to ambient pressure, referred to as the static pressure drop, are used to automatically control the system. The present invention enables adjustment of the sample fluid flow rate while maintaining a constant total fluid flow through the flow cell, and further, enables pausing the system without significant fluctuations in the vacuum.



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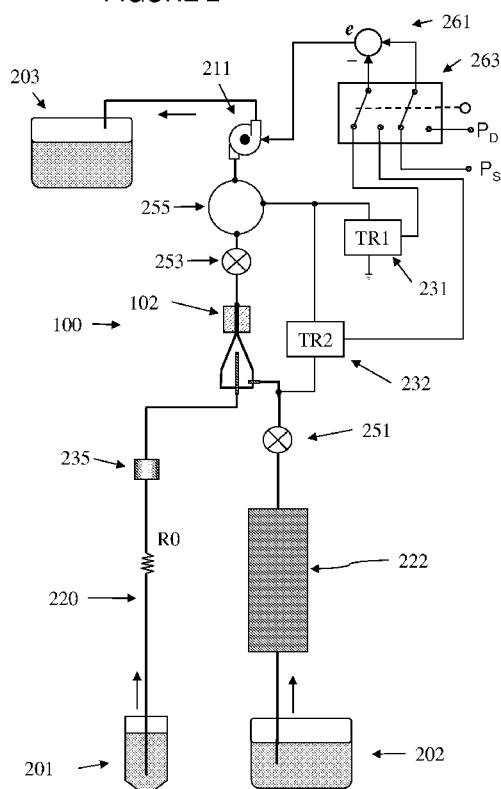
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(54) Title: DUAL FEEDBACK VACUUM FLUIDICS FOR A FLOW-TYPE PARTICLE ANALYZER

FIGURE 2



(57) Abstract: The present invention relates to a vacuum-driven fluidic system for a flow-type particle analyzer. The system includes a vacuum pump which creates a pressure drop downstream of the flow cell, which pulls sheath fluid and sample fluid through the flow cell. A variable-resistance fluidic resistor is configured to control the ratio of sample fluid flow to sheath fluid flow. Dual feedback circuits, one configured to modulate the vacuum pump power in response to the pressure drop across the flow cell, referred to as the dynamic pressure drop, and a second configured to modulate the vacuum pump power in response to the pressure drop created by the vacuum pump relative to ambient pressure, referred to as the static pressure drop, are used to automatically control the system. The present invention enables adjustment of the sample fluid flow rate while maintaining a constant total fluid flow through the flow cell, and further, enables pausing the system without significant fluctuations in the vacuum.



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DUAL FEEDBACK VACUUM FLUIDICS FOR A FLOW-TYPE PARTICLE ANALYZER

BACKGROUND OF THE INVENTION.

5 FIELD OF THE INVENTION

The present invention relates to instruments for the analysis of particles in a fluid, and their use.

DESCRIPTION OF RELATED ART

10 Flow-type particle analyzers, such as flow cytometers, are well known analytical tools that enable the characterization of particles on the basis of optical parameters such as light scatter and fluorescence, or by electrical properties, such as impedance. In a flow cytometer, for example, particles, such as molecules, analyte-bound beads, or individual cells, in a fluid suspension are passed by a detection region in which the particles are exposed to an
15 excitation light, typically from one or more lasers, and the light scattering and fluorescence properties of the particles are measured. Particles or components thereof typically are labeled with fluorescent dyes to facilitate detection, and a multiplicity of different particles or components may be simultaneously detected by using spectrally distinct fluorescent dyes to label the different particles or components. Typically, detection is carried out using a
20 multiplicity of photodetectors, one for each distinct dye to be detected. Both flow and scanning cytometers are commercially available from, for example, BD Biosciences (San Jose, CA). A description of flow cytometers is provided in Shapiro, 2003, Practical Flow Cytometry, 4th ed. (John Wiley and Sons, Inc. Hoboken, NJ), and in the references cited therein, all incorporated herein by reference.

25 In a typical flow cytometer, the particle-containing sample fluid is surrounded by a particle-free sheath fluid that forms an annular flow coaxial with the sample fluid as it passes through the detection region, thereby creating a hydrodynamically focused flow of particle-containing sample fluid in the center of the fluid stream, surrounded by particle-free sheath fluid. Typically, the ratio of sheath fluid to sample fluid is high, with the sample fluid
30 forming only a small fraction of the total fluid flow through the detection region.

Typically, flow cytometer systems have been implemented using pressure-driven fluidics in which the sample and sheath fluid are provided to a flow cell, which contains the detection region, under a pressure greater than ambient pressure. Changes in the flow rate through the flow cell of a pressure-driven fluidics system are achieved by varying the pressure in the sample tube and/or the sheath fluid reservoir that feed into the flow cell. The ratio of sample fluid to sheath fluid flowing through the flow cell is governed both by the pressure levels in the sample tube and sheath fluid reservoir, and by the ratio of the resistances of the sample fluid and sheath fluid paths.

Alternatively, flow cytometer systems have been implemented using vacuum-driven fluidics in which a vacuum pump draws a vacuum downstream of the flow cell, and the sample and sheath fluids are held at ambient pressure. Changes in the flow rate through the flow cell of a vacuum-driven fluidics system are achieved by varying the vacuum drawn by the vacuum pump, and the ratio of sample fluid to sheath fluid flowing through the flow cell is governed by the ratio of the resistances of sample fluid and sheath fluid paths.

In general, the design of pressure-driven fluidics systems is more complicated than is the design of vacuum-driven fluidics systems because of the need for components, including tubing, connections, and seals, that withstand high system pressure levels. In contrast, in a vacuum-driven flow cytometry system, the design of the fluidic connections to the sample tube and sheath fluid supply reservoir is greatly simplified as it does not require the use of pressurizable tubings, connections, and seals. The elimination of pressurized sample tubes further facilitates the design of auxiliary equipment, such as automatic tube lifters and robotic sample loaders.

U.S. Patent No. 5,395,588, incorporated herein by reference, describes a vacuum control system for use in a flow cytometer. The system includes a vacuum pump that pulls a sheath fluid from an open supply reservoir through a flow cell wherein cell analysis occurs, and discharges the flow cell effluent to an open waste reservoir. A pressure drop is created through the conduit leading from the supply reservoir to the flow cell, which also aspirates a sample consisting of a particle (e.g., cell) suspension from an open sample vessel into and through the flow cell. The flow rate of the system is regulated by monitoring the vacuum level at the outlet of the flow cell. A control circuit coupled to the vacuum sensor adjusts the electric power applied to the vacuum pump motor to maintain a predetermined vacuum level at the outlet of the flow cell.

BRIEF SUMMARY OF THE INVENTION.

The present invention provides an improved vacuum-driven fluidics system for a flow-type particle analyzer in which two or more fluidic sources, such as a sample fluid and a sheath fluid, are combined by the system just prior to analysis, such as in a flow cytometer.

5 The vacuum-driven fluidics system of the present invention, as used in a flow cytometer, includes a vacuum pump that develops a vacuum that draws sheath fluid from a sheath reservoir and sample fluid containing the particles to be analyzed from a sample tube through a flow cell, wherein analysis of the particles is carried out. Waste effluent, which is the mixture of sample and sheath fluids exiting the flow cell, is drawn through the pump and
10 discharged into a waste reservoir. A pressure sensor (pressure transducer) is configured to measure the pressure drop across the flow cell, referred to herein as the dynamic pressure drop. A first control feedback circuit, referred to herein as the dynamic control feedback circuit, is provided that enables regulating the dynamic pressure drop by modulating the vacuum pump in response to the measured dynamic pressure drop.

15 In preferred embodiments, the vacuum-driven fluidics system further includes a second pressure sensor (pressure transducer) configured to measure the vacuum relative to the ambient pressure drawn by the vacuum pump, referred to herein as the static pressure drop. A second control feedback circuit, referred to herein as the static control feedback circuit, is provided that enables regulating the static pressure drop by modulating the vacuum
20 pump motor in response to the measured static pressure drop. The control circuits allow selection of either the first, dynamic, or the second, static, control feedback circuit, such that the vacuum pump motor may be modulated in response to either the dynamic pressure drop or the static pressure drop. The function of the two feedback control circuits is described further below.

25 Preferably, the vacuum pump is modulated to control the amount of vacuum drawn by the pump by modulating the electrical power provided to the pump motor. Alternatively, the vacuum pump can be modulated to control the amount of vacuum drawn using one or more adjustable valves or other fluidic resistors that restrict the flow of fluid through the pump.

In preferred embodiments, the vacuum-driven fluidics system of the present invention
30 further includes a variable-resistance fluidic resistor in the sheath fluid path positioned between the sheath fluid reservoir and the flow cell. By varying the resistance of the variable-resistance fluidic resistor, the relative proportion of sheath fluid and sample fluid

drawn through the flow cell can be modulated. Equivalently, the sample fluid flow rate can be modulated by changing the resistance of the sheath fluid path while maintaining a constant total flow rate through the flow cell.

Alternatively, the vacuum-driven fluidics system of the present invention further
5 includes a variable-resistance fluidic resistor in the sample fluid path positioned between the sample fluid tube and the flow cell. The variable-resistance fluidic resistor in the sample fluid path also may be used in conjunction with a variable-resistance fluidic resistor in the sheath fluid path. In general, it is preferable to control the ratio of sample to sheath fluid using a variable-resistance fluidic resistor in the sheath fluid path. In a typical flow
10 cytometer, the flow of sheath fluid is on the order of 1,000 times the flow of sample fluid (typical sheath fluid flow is on the order of milliliters per minute; typical sample fluid flow is on the order of microliters per minute), and it is easier to control the flow of sheath fluid with precision.

An advantage of the vacuum-driven fluidics system of the present invention is that the
15 sample fluid flow rate can be modulated while maintaining a constant total flow rate through the flow cell. The total flow rate is held constant using the first (dynamic) feedback control loop, modulating the power of the vacuum pump to provide a constant dynamic pressure drop, as measured by first pressure sensor. In contrast, previously described flow cytometers using vacuum-driven fluidics, such as those described in US Patent No. 5,395,588, only
20 measured and controlled the static pressure drop. A constant static pressure drop provides a constant flow rate through the cuvette only if the fluidic resistances of the sample and sheath paths upstream of the flow cell are constant. A change in the sample flow rate in a vacuum-driven fluidic system that monitors only the static pressure drop would require extensive recalibration of the required static pressure drop.

25 In some embodiments of the invention, the variable-resistance fluidic resistor is configured to provide a plurality of discrete resistance levels. Preferably, this is achieved by providing alternative selectable fluid paths, each fluidic path having a different fluidic resistance. The fluid paths may be a conduits (e.g., lengths of tubing) having different lengths or diameters. Valves are situated in the sheath fluid path to allow selection of a
30 desired fluid path from among the plurality of alternative fluid paths.

In alternative embodiments of the invention, the variable-resistance fluidic resistor is continuously variable. In preferred embodiments, the sheath fluid path includes a conduit

composed of an at least partially compressible or deformable material, such as length of plastic tubing, and an adjustable pressure is applied to the outside of the tubing. Modulation of the pressure applied to the outside of the tubing changes alters the diameter and/or shape of the tubing, thereby changing the cross-sectional area of the fluidic path and, concomitantly, changing the fluidic resistance of the tubing.

The continuously variable variable-resistance fluidic resistor may consist of a length of tubing that is compressed mechanically. For example, the tubing may be wound around a cylindrical post and compressed between plates, at least one movable, having surfaces perpendicular to the post. Alternatively, the continuously variable variable-resistance fluidic resistor may consist of a length of tubing that passes through the interior of a pressure chamber having an adjustable internal pressure. The internal pressure of the pressure chamber may be modulated by connecting the chamber to adjustable pressure source, such as a compressed air source, or by altering the size and/or shape of the pressure chamber, such as by mechanical means.

The modulation of the resistance of the variable-resistance fluidic resistor can be put under automated control using servomechanisms to effect changes in the resistance settings.

The flow of sample and sheath through the system can be paused to allow, for example, a change to a new sample source after each sample analysis. In the present system, the flow of fluid may be paused by closing a valve situated in the fluid path between the flow cell and the pump. When this valve is closed, the dynamic pressure drop drops to zero, the dynamic feedback loop, which is between the dynamic pressure drop and the pump, is stopped, and the static feedback loop, which is between the static pressure drop and the pump, is activated. The static feedback loop enables maintaining the static pressure drop at a constant level during the paused state, preferably maintaining it at the static pressure drop of the system that existed while in the running state prior to pausing the system (while under control of dynamic feedback loop). When the flow of fluid through the flow cell is restarted, control of the pump is switched back to the dynamic feedback loop, which enables re-establishing and maintaining the flow across the flow cell at the same rate as it was prior to pausing the system, regardless of any changes made to the resistance level of the variable-resistance fluidic resistor while the system was paused. This switching between feedback control circuits eliminates large fluctuations in the vacuum during transitions between

running and paused states, while maintaining a constant flow rate through the flow cell for all samples.

A constant flow rate through the flow cell, or more specifically, through the cuvette within a the flow in which cell analysis takes place, is particularly important in a multi-laser flow cytometer. A multi-laser flow cytometer typically has multiple spatially separated
5 detection regions which the particles pass through as they flow through the cuvette. In order to match up the signals detected in each of the detection regions such that all signals from the same particle can be identified as coming from the particle, the transit time from one detection region to the next must be determined. Typically, using a two laser system, the
10 signals measured after excitation with the first laser in the first detection region are held in an electronic circuit until the signals measured after excitation with the second laser in the second detection region have been measured, and the two signals are then sent together for further analysis. The time between arrival of the first signal and arrival of the second signal, often referred to as a “laser delay”, depends on the distance between the detection regions and
15 on the flow rate. Similarly, in multi-laser system having more than two lasers, each of the signals from the same particle are stored until the last signal is measured, and the multiple signals are then passed on to the downstream electronics for further analysis. The vacuum-driven fluidic system of the present invention enables maintaining a constant flow rate through the cuvette, which insures constant laser delays, while allowing the sample flow rate
20 to be altered.

BRIEF DESCRIPTION OF THE SEVERAL VIEWS OF THE DRAWINGS

Figure 1 provides a schematic representation of elements of a flow cell from a typical flow cytometer. The direction of fluid flow in figure 1 is from the top of the page towards the
25 bottom.

Figure 2 provides a schematic representation of a vacuum-driven fluidic system of the present invention. The direction of fluid flow in figure 2 is from the bottom of the page towards the top, and flow cell **100** is shown in an orientation that is inverted relative its orientation in figure 1.

Figure 3 provides a schematic representation of a variable-resistance fluidic resistor of the present invention. The variable-resistance fluidic resistor provides multiple, valve-selectable, discrete fluidic resistance levels.

Figures 4a and 4b provide schematic representations of a continuously variable-resistance fluidic resistor of the present invention.

Figure 5 provides a schematic representation of an alternative embodiment of the continuously variable-resistance fluidic resistor of the present invention.

5 Figure 6 provides a schematic representation of elements of an alternative embodiment of a vacuum-driven fluidic system of the present invention having a continuously variable-resistance fluidic resistor under the control of a feedback circuit that modulates the resistance in response to the sample fluid flow rate, as measured by a flow meter in the sample fluid line.

10

DETAILED DESCRIPTION OF THE INVENTION.

The following definitions are provided for clarity. Unless otherwise indicated, all terms are used as is common in the art. All reference cited herein, both supra and infra, are incorporated herein by reference.

15

A “flow-type particle analyzer” is used herein to refers to any instrument that analyzes particles suspended in a flowing fluid stream by passing the particles past one or more optical detectors, and includes, for example, analyzing or sorting flow cytometers, hematology analyzers, and cell counters. A flow-type particle analyzer contains at least two fluid sources, and the two fluid are combined by the system just prior to analysis. For
20 example, a flow cytometer of the present invention analyzes particles suspended in a sample fluid that is hydrodynamically focused by a sheath fluid.

Sheath fluid refers to a substantially particle-free fluid that is used to surround the particle-containing sample fluid to achieve hydrodynamic focusing, as commonly practiced in a flow cytometer.

25

The terms “pressure sensor”, “pressure transducer”, “vacuum sensor”, “vacuum transducer”, and “transducer”, with reference to measuring pressure, are all used interchangeably herein.

A fluidic “line”, as used herein, refers to a fluid conduit or channel for transporting fluid. Typically, the sample fluid line and sheath fluid line will consist primarily of lengths
30 of tubing, although the lines may include valves and additional fluidic resistors.

Pressure Transducers

A typical pressure sensor incorporates a diaphragm of a piezoresistive material which generates a proportional voltage when deflected in response to a pressure or vacuum level. Suitable pressure sensors are known in the art and are commercially available from, for example, Honeywell Corporation (Morristown, NJ). Examples include the Honeywell 26PC and 140PC series differential vacuum sensors and Sensym SDX pressure sensors.

Variable-resistance Fluidic Resistors

In preferred embodiments, the vacuum-driven fluidics system of the present invention further includes a variable-resistance fluidic resistor in either the sample fluid path between the sample tube and the flow cell, in the sheath fluid path position between the sheath fluid reservoir and the flow cell, or both. Preferably, the variable-resistance fluidic resistor is incorporated into the sheath fluid path, as exemplified, below. By varying the resistance of the variable-resistance fluidic resistor, the relative proportion of sheath fluid and sample fluid drawn through the flow cell can be modulated. As the total flow rate through the flow cell is held constant, modulation of the relative proportion of sheath fluid and sample fluid drawn through the flow cell also controls the sample fluid flow rate through the flow cell.

Preferably, the variable-resistance fluidic resistor is a viscously dominated restrictor, which facilitates balancing the pressures in the rest of the viscously dominated fluid circuit. In preferred embodiments, a viscously dominated restrictor is achieved by using a length of tubing or similar conduit having essentially a constant internal diameter. The resistive force, for a fluid of a given viscosity, depends on the length and internal cross-sectional area of the conduit, and the length is selected to provide the desired resistance. In contrast, simply pinching a tubing at a single point, or using a valve (such as a needle valve) to provide a flow restriction, results in a convective acceleration. Although this provides variable-resistance, it is less desirable in a viscously dominated system. Due to the effects of temperature on viscosity, the temperature dependence of the resistance of the sheath fluid line incorporating the viscously dominated fluidic resistor is the same as the temperature dependence of the resistance of the sample fluid line. Thus, the ratio of the sample fluid line and sheath fluid line resistances remains the same as the temperature is varied. In contrast, as pinching is convectively dominated and the resistance is not a function of temperature, the use of a

pinching-type resistance would result in a change in the ratio of the path resistances with a change in temperature.

Typically, the conduit consists of a length of a glass, plastic, or steel tubing. Suitable tubing is available commercially in a variety of diameters. Typically, the diameter will be selected such that the desired flow resistance can be achieved with a convenient length of tubing, and then minor adjustments to the flow resistance will be made by modifying the length of the tubing. The diameter and length of the tubing will be selected based on the application, following the guidance herein.

A variable-resistance fluidic resistor may provide a choice between a plurality of discrete resistance settings. Alternatively, a variable-resistance fluidic resistor may provide a continuously adjustable resistance. Examples of different variable-resistance fluidic resistors are described below and in the figures.

Variable-resistance fluidic resistors that provide alternative discrete levels of fluidic resistance preferably are implemented by providing multiple, valve-selectable, parallel fluidic channels, each providing a distinct fluidic resistance. Alternative total fluidic resistance levels of the variable-resistance fluidic resistor, as a whole, are achieved by selecting which of the alternative internal fluidic channels are available for flow through the variable-resistance fluidic resistor.

Variable-resistance fluidic resistor that provide a continuously variable resistance are preferably implemented by providing a length of at least partially compressible or deformable material, such as length of plastic tubing, and a means for applying an adjustable pressure to the outside of the tubing. The tubing is selected such that the uncompressed tubing provides the lowest level of resistance desired. An increase in the pressure applied to the outside of the tubing will change alters the diameter and/or shape of the tubing, thereby increasing the fluidic resistance.

Description based on the figures**Figure 1**

Figure 1 depicts a schematic representation of elements of a typical flow cytometer useful with the fluidic system of the present invention. Flow cell **100** includes flow cell chamber **106**, sample inlet port **108**, and a sheath inlet port **110**. The sample inlet port **108** and sheath inlet port **110** are adapted to provide particle-containing fluid sample and particle-free sheath fluid, respectively, into the flow cell chamber **106**. Flow cell chamber **106** converges to an opening that is joined to cuvette channel **104**, which passes through cuvette **102**.

In use, sample fluid containing the particles to be analyzed is introduced into the flow cell **100** through sample inlet port **108**, and particle-free sheath fluid is introduced into the flow cell through sheath inlet port **110**. Fluids exit through cuvette channel **104** and are directed to a waste receptacle (not shown). The flow cell is designed such that the sheath fluid forms an annular flow coaxial with the sample fluid, thereby creating a hydrodynamically focused flow of particle-containing sample fluid in the center of the fluid stream, surrounded by particle-free sheath fluid, as the fluid convectively accelerates through the converging path of the flow cell. The combined fluid stream consisting of sheath fluid and sample fluid is referred to herein as the “sample stream”, “flow stream” or “particle stream”.

Optical analysis of the particles within the sample stream is carried out by exposing the sample stream in detection region **120** to excitation light from one or more excitation light sources and detecting light emanating from the detection region **120** using one or more photodetectors (not shown). Cuvette **102** is constructed, at least in part, from an optically clear material to enable optical excitation and detection. Figure 1 depicts the use of two excitation light sources. Excitation light source **118** emits a first beam of light that is focused by lens **116** onto the sample stream at a first interrogation point within detection region **120**. Excitation light source **119** emits a second beam of light that is focused by lens **116** onto the sample stream at a second interrogation point within detection region **120**, wherein the second interrogation point is downstream of the first interrogation point by a distance **122**. A mirror or beam-splitter **117** is used to redirect the second beam to be essentially parallel the first beam at the interrogation points.

Typically, for each of the multiple excitation light sources, multiple detectors (not shown) are present to detect fluorescent light emitted from particles in the sample stream, each detector configured to detect emitted light within a defined range of wavelengths. In addition, additional detectors are positioned to detect excitation light from at least one
5 excitation light source that is scattered by particles at a low angle relative to the excitation beam, referred to as forward scatter light, and excitation light that is scattered by particles at nearly right angles to the excitation beam, referred to as side scatter light. Suitable photodetectors for use in a flow-type particle analyzer include, for example, photomultiplier tubes (PMTs), avalanche photo diodes, photodiodes, or any other suitable light-detecting
10 device.

The spatial separation of the interrogation points allows for the particles to be exposed to each of the excitation lights, which are of distinct wavelengths, separately. As the particles move through the cuvette channel **104**, they are first exposed to the excitation light from excitation light source **118** at the first interrogation point. The particles then move out of the
15 first interrogation point and into the second interrogation point where they are exposed to the excitation light from excitation light source **119**. The time it takes for a particle to move from the first interrogation point to the second interrogation point is referred to herein as the “laser delay”.

The laser delay is an important parameter that is used to electronically match up
20 signals obtained from the emissions of a particle exposed to the first excitation light with signals from the emissions of the same particle exposed to the second excitation light, so that that the signals are all identified as originating from the same particle. The laser delay, for a given distance **122** between interrogation points, depends entirely on the flow rate through the cuvette channel **104**. For at least this reason, the flow rate through the flow cell should be
25 maintained constant during the analysis of sample particles.

The flow rate through the flow cell can be measured by analyzing a sample of test particles that are detectable at each interrogation point. For each particle, the time between the signals obtained from the emissions of the particle exposed to the first excitation light and the signals from the emissions of the particle exposed to the second excitation light is
30 measured. As the distance **122** between interrogation points is known from the design of the instrument, the time delay between the first and second signals enables calculation of the flow rate through the detection region **120**. Alternatively, the flow rate can be measured by

measuring the accumulation of fluid downstream of the flow cell over a specified period of time.

Figure 2

Figure 2 depicts a schematic representation of elements of a fluidic system of the present invention. A system vacuum is developed by a vacuum pump **211**, which draws sheath fluid from the sheath reservoir **202** and sample fluid containing the particles to be analyzed from the sample tube **201** through flow cell **100**, wherein optical analysis is carried out (optics not shown). Waste effluent, which is the mixture of sample and sheath fluids exiting the flow cell, is discharged into waste reservoir **203**.

Pulsations in the vacuum developed by vacuum pump **211**, which typically is a diaphragm-type pump, are attenuated by accumulator **255**, also referred to as a pulsation damper. The accumulator can be a sealed canister with an internal volume many times (e.g., 10 to 1000 times) the stroke volume of the vacuum pump.

Transducer **231** measures the pressure drop developed by vacuum pump **211** relative to atmospheric pressure. This pressure drop is referred to herein as the “static pressure drop”. The static pressure drop preferably is measured from the interior of accumulator **255** so that a stable measurement is obtained.

Transducer **231** typically is connected to accumulator **255** by a short tube, such that the pressure in the tube equals the pressure in the accumulator. It is desirable to include an air bleed (e.g., a small orifice connecting the interior of the tube to the outside air) in the tube connecting transducer **231** and accumulator **255**, positioned near the transducer, to allow a small amount of air to be drawn into and through the tube, drawn by the vacuum in the accumulator. The air bleed should be small enough such that the flow of air through the tube has an insignificant effect on the measurement of the static pressure drop. The minor air flow through the tube in the direction from the orifice (near the transducer) towards the accumulator prevents any fluid or foam that may be present in the accumulator from entering the tube to the transducer, which could affect the accuracy of the measurement.

Transducer **232** measures the pressure drop across the cuvette **102** (measured from upstream of the flow cell to the accumulator **255**). This pressure drop is referred to herein as the “dynamic pressure drop”. For a given total flow rate through the cuvette, the dynamic pressure drop is constant. Thus, by modulating the power of the vacuum pump **211** to

provide a constant dynamic pressure drop, a constant total flow rate through the cuvette can be maintained.

Sample fluid is drawn through sample line **220** and into flow cell **100** through sample inlet port **108** (shown in figure 1). This entire sample path has a fluid resistance **R0**.

5 Sheath fluid is drawn through a variable-resistance fluidic resistor **222** and into flow cell **100** through sheath inlet port **110** (shown in figure 1). In a preferred embodiment, the fluidic resistance of the variable-resistance fluidic resistor is adjustable to multiple, discrete fluidic resistance settings. In another embodiment, the fluidic resistance of the variable-resistance fluidic resistor is continuously adjustable over a predefined range.

10 The relative proportions of sample fluid and sheath fluid that are drawn into flow cell **100** depend on the ratio of the sample line fluidic resistance **R0** and the fluidic resistance of the variable-resistance fluidic resistor **222**. Thus, by modulating the fluidic resistance of the fluidic resistance of the variable-resistance fluidic resistor **222**, the ratio of sample fluid to sheath fluid can be controlled. If the total flow rate through the flow cell is held constant by
15 maintaining a constant dynamic pressure drop, each reduction of the effective fluidic resistance of variable-resistance fluidic resistor **222** results in a decrease in the sample fluid flow rate and an increase in the sheath fluid flow rate. Thus, a desired sample flow rate can be selected by an appropriate modulation of the total fluidic resistance of the variable-resistance fluidic resistor **222**, while maintaining a constant flow rate through the flow cell.

20 Valve **253** enables shutting off the fluid flow through the flow cell completely. The paused to allow, for example, a change to a new sample source after each sample analysis. In the present system, the flow of fluid may be paused by closing a valve situated in the fluid path between the flow cell and the pump. When this valve is closed, the dynamic pressure drop drops to zero, the first feedback loop, which is between the dynamic pressure drop and the pump, is stopped, and the second feedback loop, which is between the static pressure drop
25 and the pump, is activated. The second feedback loop enables maintaining the static pressure drop at a constant level during the paused state, preferably maintaining the static pressure drop of the system that existed while in the running state prior to pausing the system (while under control of first feedback loop). When the flow of fluid through the flow cell is
30 restarted, control of the pump is switched back to the first feedback loop, which enables maintaining a constant flow across the flow cell even after changes in the sample flow rate. This switching between feedback control circuits eliminates large fluctuations in the vacuum

during transitions between running and paused states, while maintaining a constant flow rate through the flow cell for all samples.

Valve **251** enables shutting off the sheath fluid flow completely. Valve **251** is used to temporarily stop the sheath fluid flow and temporarily increase (“boost”) the sample fluid flow rate following connection of the sample tube **201** to the sample line **220**, in order to shorten the time it takes to draw sample fluid to the flow cell **100**. When the sample fluid reaches the flow cell, valve **251** is opened, the flow of sheath fluid establishes a hydrodynamically focused stream, and the sample and sheath fluid flow rates return to the desired rates for analysis. Valves **251** and **253** preferably will be under automatic control in a coordinated manner, such that valve **253** can be opened for a predetermined time prior to opening valve **251** in order to permit a vacuum to be developed in said flow cell before opening said valve **251**.

Controller **261** with switching mechanism **263** controls the switching between the modulation of the power of vacuum pump **211** to provide a constant dynamic pressure drop and modulation of the power of vacuum pump **211** to provide a constant static pressure drop. To maintain a constant dynamic pressure drop, the controller compares the dynamic pressure drop measured by transducer **232** to a stored desired dynamic pressure drop P_D . The desired dynamic pressure drop P_D is determined during instrument setup as the dynamic pressure drop that provides the desired flow rate through the flow cell. To maintain a constant static pressure drop, the controller compares the dynamic pressure drop measured by transducer **231** to a stored desired static pressure drop P_S . The desired static pressure drop P_S is the measured static pressure drop that corresponds to the instrument running with the desired flow rate through the flow cell, which depends on the selected setting of the variable-resistance fluidic resistor. Multiple values for the desired static pressure drop P_S may be stored, each corresponding to a predefined resistance setting of the variable-resistance fluidic resistor. Alternatively, the desired static pressure drop P_S may be stored immediately before pausing the system, and the system restarted with the same resistance setting of the variable-resistance fluidic resistor that was in effect just prior to pausing the system.

Preferably, automatic control of the pressure drop feedback circuits (through controller **261**) and of valves **251** and **253**, will be provided in a coordinated manner.

Flow sensor **235** is positioned on sample line **220** to provide a direct measure of the sample fluid flow rate. Suitable high precision liquid flow sensors and liquid flow meters

with measurement ranges down to nanoliters per minute are commercially available from, for example, Sensirion Inc. (Westlake Village, CA). Flow sensor **235** is optional, but facilitates setting up the flow system. During instrument setup (system calibration), the fluidic resistance of variable-resistance fluidic resistor **222** is adjusted to provide the desired ratio of sheath to sample fluid, and the flow sensor provides an independent measure of the resulting sample fluid flow rate. Alternatively, the flow rate of the sample fluid can be measured by other means, such as by analyzing a sample containing a known concentration of test particles. By measuring the rate of detection of the test particles, the flow rate in the sample line **220** can be inferred.

The adjustment of the fluidic resistance of variable-resistance fluidic resistor **222** during instrument calibration to obtain a desired sample fluid flow rate can be automated, as described, below, with reference to figure 6.

Figure 3

Figure 3 depicts a schematic representation of an embodiment of a variable-resistance fluidic resistor designed to provide alternative discrete levels of fluidic resistance. Within the variable-resistance fluidic resistor are multiple parallel fluidic channels, each providing a distinct fluidic resistance, and the alternative total fluidic resistance levels of the variable-resistance fluidic resistor, as a whole, are achieved by selecting which of the alternative internal fluidic channels are available for flow through the variable-resistance fluidic resistor.

Variable-resistance fluidic resistor **320** contains internal fluid channels **321**, **322**, and **323**, which provide fluidic resistances **R1**, **R2**, and **R2**, respectively. The selection of which of the three parallel fluid channels are available for sheath fluid flow is controlled by two-way valve **355**, which controls the flow through fluid channel **322**, and two-way valve **356**, which controls the flow through fluid channel **323**. Fluid channel **321** is always open for sheath fluid flow. The maximum resistance of the variable-resistance fluidic resistor **320** is provided by flow through the single fluid channel **321**, selected by closing both valves **356** and **355**. Opening one or the other, or both, of the valves provides at least one fluid channel in parallel to fluid channel **321**, which decreases the total fluidic resistance through the variable-resistance fluidic resistor **320**.

Although variable-resistance fluidic resistor **320** contains three internal fluid channels, it will be clear that essentially any number of discrete levels of fluidic resistance can be

achieved using a multiplicity of alternative parallel fluidic channels, each with a defined fluidic resistance, and valves to enable selection of the fluidic channels. In general, the equivalent resistance of a circuit having a set of N resistors in parallel is related to the resistance values of the constituent parallel channels as follows:

5

$$\frac{1}{R} = \sum_{i=1}^N \frac{1}{R_i} ,$$

wherein R is the equivalent resistance of a circuit, and each R_i is the resistance of parallel channel I , and the summation is over all the N parallel channels.

10

The equivalent resistances of variable-resistance fluidic resistor **320** through the parallel circuit, from the point that internal fluid channels **321**, **322**, and **323** diverge until these internal fluid channels rejoin, for each of the option fluid paths defined by valves **356** and **355** are shown in the table, below.

15

Effective Resistance of Fluidic Resistor **320**

Valve 356	Valve 355	Total Resistance
closed	closed	R_1
open	closed	$1/(1/R_1 + 1/R_2)$
closed	open	$1/(1/R_1 + 1/R_3)$
open	open	$1/(1/R_1 + 1/R_2 + 1/R_3)$

Each reduction of the effective fluidic resistance of variable-resistance fluidic resistor **320** results in an increase in the ratio of sheath to sample fluid flowing through the flow cell. If the total flow rate through the flow cell is held constant by maintaining a constant dynamic pressure drop, each reduction of the effective fluidic resistance of variable-resistance fluidic resistor **320** results in a decrease in the sample fluid flow rate. Thus, a desired sample flow rate can be selected by an appropriate modulation of the total fluidic resistance of the variable-resistance fluidic resistor, while maintaining a constant flow rate through the flow cell.

The total sheath fluid path from the sheath reservoir **202** to the flow cell **100** (shown in figure 2) includes sheath fluid line **324**, having resistance **R4**, variable-resistance fluidic resistor **320**, and sheath fluid line **325**, having resistance **R5**. The total resistance of the sheath fluid path is the sum of the resistances of these three components, **R4 + R5** + the
5 resistance of the variable-resistance fluidic resistor **320**. Typically, the variable-resistance fluidic resistor **320** will provide the majority of the total resistance of the sheath fluid path.

Figure 4

Figures 4a and 4b depict two views of a schematic representation of an alternative
10 embodiment of a variable-resistance fluidic resistor wherein the resistance is continuously variable. In this embodiment, the modulation of the fluid resistance is achieved by compressing a length of tubing, thereby changing the inside diameter.

Sheath fluid line **421** is a compressible tubing, such as a peristaltic pump tubing. A section of the sheath fluid line **421** is coiled around center post **464** and positioned inside a
15 cylindrical base housing **460**. Holes in the base housing allow the tubing to enter and exit the base housing without being pinched. A circular top plate **464** is positioned inside the top opening of the base housing so as to form a cylindrical cavity containing the coil of sheath fluid line **421**. Top plate **462** contains a whole that allows center post **464** to extend through
20 top plate **462** such that the top plate can slide down into the base housing. The center post is threaded at the upper end, and a nut **466** is screwed onto the end of the center post. Tightening the nut presses top plate **462** onto the top of the coil of the sheath fluid line **421** compressing the sheath fluid line and increasing the fluidic resistance.

The fluidic resistance of sheath fluid line **421** is continuously variable, controlled by the force applied by the nut **466**, and precise control over the change in resistance is possible.
25 The tubing diameter and the number of windings in the coil will be selected to provide the range and control required for the particular application. The flow path of the sheath fluid is very simple, can be flushed easily for cleaning, and has no internal edges or other structures that might collect cells or particles.

It will be clear that the modulation of the fluidic resistance of the variable-resistance
30 fluidic resistor can be automated to provide remote control of the fluidic resistance.

Figure 5

Figure 5 depicts a schematic representation of an alternative embodiment of a variable-resistance fluidic resistor wherein the resistance is continuously variable. Sheath fluid line **521** is a compressible tubing, such as a peristaltic pump tubing. The sheath fluid line **521** is passed through a sealed pressurized tank **522**, which is filled with a gas or fluid under pressure through inlet port **525**. Changes in the pressure within the tank compress the sheath line, changing the fluidic resistance.

It will be clear that the modulation of the fluidic resistance of the variable-resistance fluidic resistor can be automated to provide remote control of the fluidic resistance.

Figure 6

Figure 6 depicts an automated feedback control circuit for automatically modulating the sample fluid flow rate to obtain a preselected sample fluid flow rate during system calibration. Continuously variable variable-resistance fluidic resistor **622** is configured to enable modulation of the fluidic resistance using a servomechanism. Examples of suitable variable-resistance fluidic resistors are as depicted in figure 4, wherein nut **466** is adjusted using a servomotor, or as depicted in figure 5, wherein modulation of the pressure source is under servomotor control. Controller **661** compares the flow rate measured by flow sensor **235** to a stored desired flow rate **FR** and modulates the fluidic resistance of variable-resistance fluidic resistor **622** until the measured flow rate matches the desired flow rate **FR**.

System calibration

In general, the initial calibration of a flow-type particle analyzer containing the vacuum-driven fluidics of the present invention preferably is carried out using the following steps:

- A. The resistance of the variable fluidic resistor is set to any convenient setting. Because the dynamic pressure drop required to maintain the desired flow rate through the flow cell is not dependent on the resistance of the continuously variable fluidic resistor, the resistance setting used as this step is not critical.
- B. The dynamic pressure drop that will obtain the desired flow rate through the flow cell is determined. The value of the dynamic pressure drop is stored and used in the feedback control system to maintain a constant dynamic pressure drop.

C. The variable-resistance fluidic resistor is adjusted to give a desired sample flow rate, while maintaining the dynamic pressure drop. The sample flow rate preferably is measured by flow-rate meter in-line with the sample fluid line, as described above. In embodiments using a discrete value variable-resistance fluidic resistor, adjustments are made
5 in step (C) to each of the discrete resistance levels to obtain each of the desired sample flow rates. Preferably, the static pressure drop corresponding to each of the sample flow rates is recorded, for use in pausing and restarting the system.

For example, using a discrete-value, variable-resistance fluidic resistor as depicted in figure 3, the variable fluidic resistor initially is configured with nominally long lengths of
10 tubing for the internal fluid channels **321**, **322**, and **323**. The adjustments in step (C) are carried out with valves **356** and **355** initially closed, such that sheath fluid travels only through fluid channel **321**. This provides the highest level of resistance to the sheath fluid, which corresponds to the highest ratio of sample to sheath fluid and, the highest sample fluid flow rate. Fluid channel **321** is adjusted by, for example, changing the length of the tubing to
15 obtain the desired “high” sample flow rate, while maintaining the dynamic pressure drop. Next, valve **356** is opened such that sheath fluid travels in parallel through fluid channels **321** and **322**. This provides a reduced level of resistance to the sheath fluid, which corresponds to reduced sample fluid flow rate. Fluid channel **322** is adjusted to give the desired “medium” sample flow rate, while maintaining the dynamic pressure drop. Next, valve **355** is opened
20 such that sheath fluid travels in parallel through fluid channels **321**, **322**, and **323**. This provides a further reduced level of resistance to the sheath fluid, which corresponds to further reduced sample fluid flow rate. Fluid channel **323** is adjusted to give a desired “low” sample flow rate, while maintaining the dynamic pressure drop. It will be clear that although the setup described above describes the setting of three discrete fluidic resistance levels, the
25 presence of two valves allows for up to four discrete fluidic resistance levels.

In embodiments using a continuously variable variable-resistance fluidic resistor, the resistance level is modulated , while maintaining the dynamic pressure drop, until the desired sample flow rate is obtained, preferably under automated control. For example, using a continuously discrete-value, variable-resistance fluidic resistor and control feedback circuit as
30 depicted in figure 6, the resistance is modulated automatically in response to the measured sample flow rate until the desired flow rate is obtained.

Pausing and Restarting the System

One aspect of the present invention is an improved method for pausing a vacuum-driven fluidic system in a flow-type fluid analyzer that facilitates maintaining a constant vacuum pump power level when switching between running and paused states. Flow of fluid through the flow cell can be stopped (i.e., the system paused) by closing valve **253**. In order to avoid fluctuations in the vacuum drawn by pump **211**, control of the vacuum pump is switched, preferably automatically, to the static pressure feedback loop to maintain the static pressure drop at the constant value that existed immediately prior to pausing the flow. The vacuum pump power level required to maintain the desired dynamic pressure drop while the system is running should equal the power level required to maintain the corresponding static pressure drop (measure just prior to pausing the system) once the system is paused. The static pressure drop just prior to pausing the flow is determined either at the time of instrument calibration, as described above, or by measuring the static pressure drop prior to closing valve **253**.

To restart the system, valve **253** is opened, allowing vacuum pump **211** to draw a vacuum through the flow cell. Control of the vacuum pump is switched, preferably automatically, to the dynamic pressure feedback loop, and the power to the pump is adjusted to maintain the dynamic pressure drop at the value determined at setup to provide the desired flow rate through the flow cell.

The system will routinely be paused to allow for replacement of the sample tube. Upon restarting, sample fluid from the new sample tube will need to be drawn through the sample fluid line before reaching the flow cell. It is desirable to speed up (boost) this initial flow of sample until the sample fluid line is full of sample fluid from the new tube.

Maximum sample fluid flow is achieved by shutting off sheath fluid flow by closing valve

251. When restarting the system, valve **253** is opened for a predetermined time, which will be based on the flow rate and volume of the sample fluid line, prior to opening valve **251** in order to permit a vacuum to be developed in the flow cell before opening valve **251**, thereby pulling sample fluid through the sample line and into the flow cell prior to opening valve **251**.

We Claim:

1. A fluidic system for a flow-type particle analyzer, comprising:

a) a flow cell having

5 a sample fluid inlet port,

a sheath fluid inlet port,

an outlet port, and

a cuvette, wherein said cuvette contains a cuvette channel having a input end
and an output end, wherein said input end is in fluidic communication with

10 said sample inlet port and said sheath fluid inlet port, and said output end is in
fluidic communication with said outlet port;

b) a sample fluid line in fluidic communication with said sample inlet port, for
providing a particle-containing sample fluid from a sample fluid container;

c) a sheath fluid line in fluidic communication with said sheath fluid inlet port, for
15 providing a sheath fluid from a sheath fluid reservoir;

d) an outlet line in fluidic communication with said outlet port;

e) a vacuum pump having a controllable power level, in vacuum communication with
said outlet line, configured to draw a vacuum in said outlet line, thereby pulling said sample
and sheath fluids through said flow cell;

20 f) a first sensor configured to measure a pressure drop from the sheath fluid inlet port
to said cuvette outlet port;

g) a first control feedback circuit configured to regulate the power of said vacuum
pump in response to the pressure drop measured by said first sensor;

h) a second sensor configured to measure a pressure drop from said cuvette outlet
25 port to atmospheric pressure;

i) a second control feedback circuit configured to regulate the power of said vacuum
pump in response to the pressure drop measured by said second sensor;

where said sample fluid line or said sheath fluid line comprises a variable-resistance
fluidic resistor.

30 2. The fluidic system of claim 1, wherein said sheath fluid line comprises a variable-
resistance fluidic resistor.

3. The fluidic system of claim 2, further comprising:

a) a first valve, positioned in line with said sheath fluid line, configured to control the flow of said sheath fluid into said flow cell;

5 b) a second valve, positioned in line with said outlet line, configured to control the flow of said sheath fluid out of said flow cell;

c) a valve controller operatively connected to said first and second valves.

4. A fluidic system of claim 2, wherein said variable-resistance fluidic resistor is configured to provide a plurality of discrete resistance levels.

10

5. The fluidic system of claim 4, wherein said variable-resistance fluidic resistor comprises a plurality of selectable fluid paths.

15 6. The fluidic system of claim 5, wherein said variable-resistance fluidic resistor further comprises a plurality of valves configured to allow section of said selectable fluid paths.

7. A fluidic system of claim 2, wherein said variable-resistance fluidic resistor is configured to provide a continuously variable fluidic resistance.

20 8. The fluidic system of claim 7, wherein said variable-resistance fluidic resistor comprises a conduit composed of an at least partially compressible or deformable material, and a controllable means for applying pressure to the outside of said conduit.

25 9. The fluidic system of claim 8, wherein said controllable means for applying pressure is configured to apply a mechanical pressure.

10. The fluidic system of claim 8, wherein said controllable means for applying pressure is configured to apply a pressure by through a fluid or gas surrounding said conduit.

30 11. The fluidic system of claim 7, further comprising:

a) a flow meter configured to measure a flow rate in said sample fluid line; and

b) a controller operatively connected to said flow meter and to said variable-resistance fluidic resistor, configured to automatically modulate the resistance of said variable-resistance fluidic resistor in response to said flow rate measured by said flow meter.