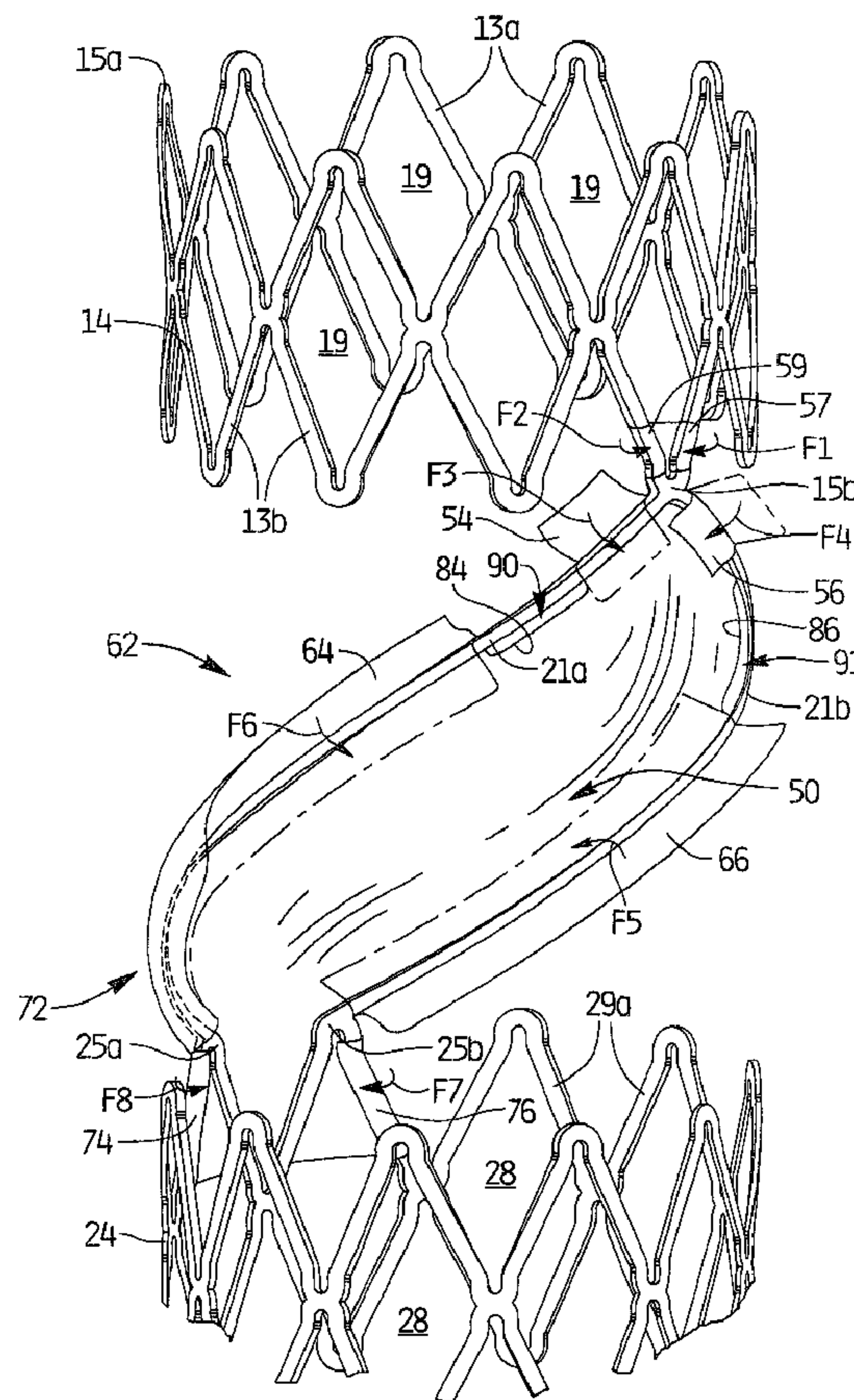




(86) **Date de dépôt PCT/PCT Filing Date:** 2009/01/02
 (87) **Date publication PCT/PCT Publication Date:** 2009/07/16
 (45) **Date de délivrance/Issue Date:** 2018/05/01
 (85) **Entrée phase nationale/National Entry:** 2010/06/30
 (86) **N° demande PCT/PCT Application No.:** US 2009/000001
 (87) **N° publication PCT/PCT Publication No.:** 2009/088957
 (30) **Priorité/Priority:** 2008/01/04 (US61/010,012)

(51) **Cl.Int./Int.Cl. A61F 2/24** (2006.01)
 (72) **Inventeurs/Inventors:**
 KALMANN, MENNO, NL;
 HINCHLIFFE, PETER W. J., US;
 LEHMAN, ADAM I., US
 (73) **Propriétaire/Owner:**
 DEEP VEIN MEDICAL, INC., US
 (74) **Agent:** BERESKIN & PARR LLP/S.E.N.C.R.L.,S.R.L.

(54) **Titre : DISPOSITIF PERMETTANT DE REGULER LA CIRCULATION SANGUINE**
 (54) **Title: DEVICE FOR REGULATING BLOOD FLOW**



(57) **Abrégé/Abstract:**

An implantable device for regulating blood flow through a blood vessel comprising an elongated support dimensioned and configured to be implanted in a blood vessel. The support includes a linking member linking axially spaced apart portions to one

(57) **Abrégé(suite)/Abstract(continued):**

another. A valve membrane extends between the axially spaced apart support portions and includes first region folded over the first linking member and attached thereto and a second region adjacent the first region and unattached to the first linking member. The second region is movable between a first position to enable blood flow and a second position to inhibit blood flow.

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property Organization
International Bureau



(43) International Publication Date
16 July 2009 (16.07.2009)

PCT

(10) International Publication Number
WO 2009/088957 A1

(51) International Patent Classification:
A61F 2/24 (2006.01)

(21) International Application Number:

PCT/US2009/000001

(22) International Filing Date: 2 January 2009 (02.01.2009)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:

61/010,012 4 January 2008 (04.01.2008) US

(71) Applicant (for all designated States except US): **INTERVENTIONAL & SURGICAL INNOVATIONS, LLC** [US/US]; 25 High Meadow Road, Campbell Hall, NY 10916 (US).

(72) Inventors: **KALMANN, Menno**; Hullenkant 45, NL-8075 PD Elspeet (NL). **HINCHLIFFE, Peter, W.J.**; 25 High Meadow Road, Campbell Hall, NY 10916 (US). **LEHMAN, Adam, I.**; 26 Hillside View Road, Northford, CT 06472 (US).

(74) Agent: **JONES, Joshua, L.**; Edwards Angell Palmer & Dodge LLP, P.O. Box 55874, Boston, MA 02205 (US).

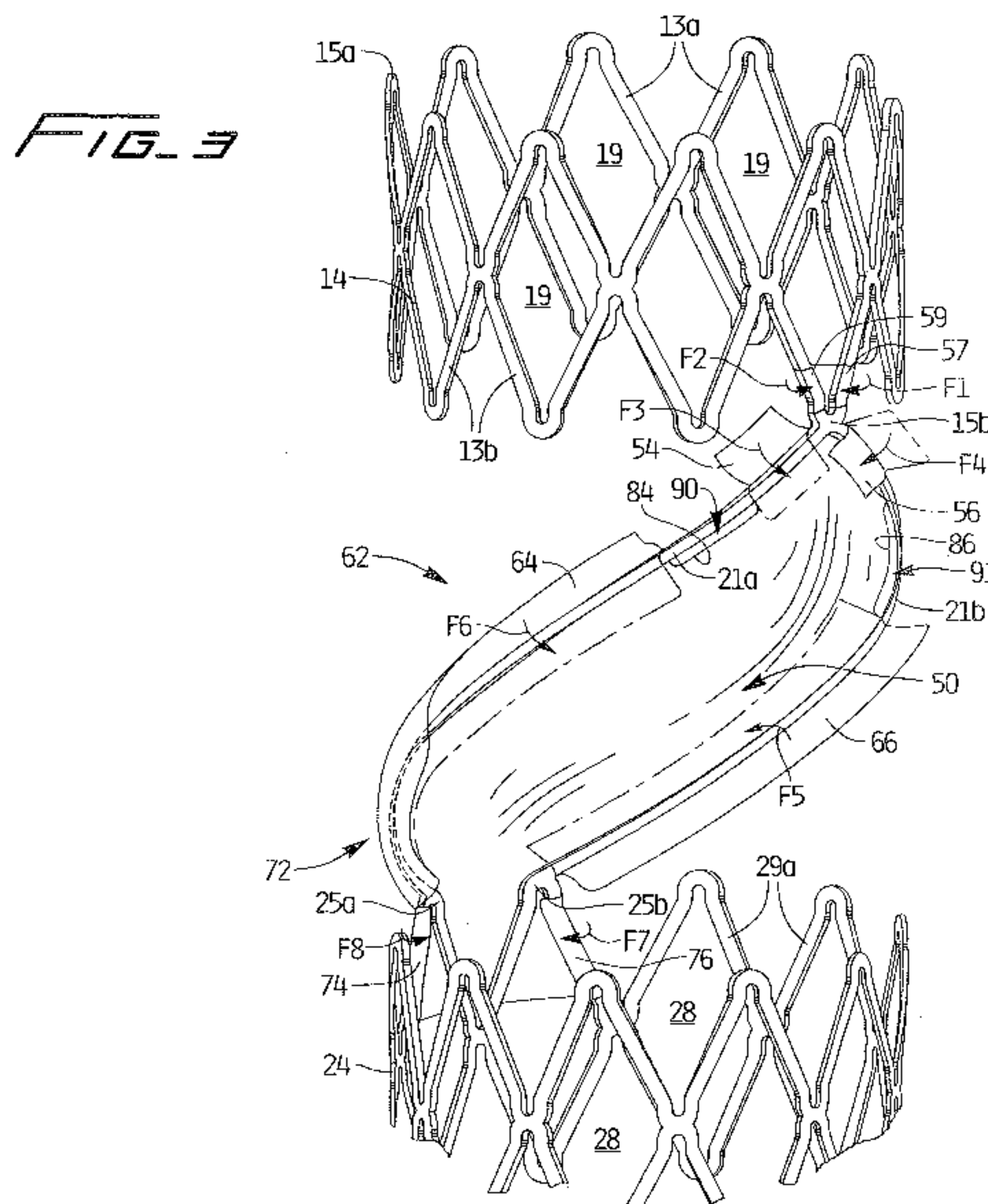
(81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AO, AT, AU, AZ, BA, BB, BG, BH, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IS, JP, KE, KG, KM, KN, KP, KR, KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RS, RU, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

(84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV, MC, MK, MT, NL, NO, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

- with international search report
- before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments

(54) Title: DEVICE FOR REGULATING BLOOD FLOW



(57) Abstract: An implantable device for regulating blood flow through a blood vessel comprising an elongated support dimensioned and configured to be implanted in a blood vessel. The support includes a linking member linking axially spaced apart portions to one another. A valve membrane extends between the axially spaced apart support portions and includes first region folded over the first linking member and attached thereto and a second region adjacent the first region and unattached to the first linking member. The second region is movable between a first position to enable blood flow and a second position to inhibit blood flow.

WO 2009/088957 A1

DEVICE FOR REGULATING BLOOD FLOW

1. Field of the Invention

5 The subject invention is directed to a device for regulating blood flow in the venous system, and more particularly, to an implantable valve device for regulating the flow of blood through a blood vessel.

2. Description of Related Art

10

The blood system, and in particular the venous blood system of the legs and arms is provided with valves that are uniquely located in a manner so as to ensure that blood will not flow back upstream in the direction from which it has been pumped from the heart. In the arms and legs, there is a deep venous system and a surface (superficial) venous system.

15

Due to various causes, thrombosis can occur in the deep venous system. Blood thinning can alleviate this problem. However, valves do not effectively close and often leak when the blood is thinned. This can cause increased venous blood pressure in the direction of the ankles, which can lead to a variety of problems including pain, swelling, varicose veins

20

and ulcers. Complaints of this type are wide spread among those who spend prolonged periods of time in a standing position, for instance, surgeons.

The surface venous system of the leg is relatively weaker than the deep venous system, and it has the tendency to spontaneously widen due to the increased pressure of blood from above. This widening prevents the valves from functioning effectively and can lead to varicose veins, which are both unattractive and painful. Major surgery is often required to treat these blood vessel problems. For example, varicose veins are treated by either closing off the vein, which leads to a reduced blood flow capacity and increased pressure on surrounding blood vessels to ensure blood drainage, or by completely removing the varicose veins, which leads to the same problem. The deep veins require invasive surgery and because of the swelling, risk of infection and trauma is seldom attempted. In either case, the treatment of the surface veins does not treat the failed valves in the deep system, thereby causing the continued pressure and back flow into the legs. The subject invention is directed to a device for obviating problems of this type.

15 SUMMARY OF THE INVENTION

The subject invention is directed to a new and useful implantable valving device for mechanically regulating blood flow through a blood vessel.

The present invention provides in one aspect an implantable device for regulating blood flow through a blood vessel comprising an elongated support dimensioned and configured to be implanted in a blood vessel and a valve membrane. The support includes axially spaced apart first and second substantially annular support portions and a first linking member linking the axially spaced apart portions to one another. The valve membrane extends between the axially spaced apart support portions and has an upper

portion, a lower portion and an intermediate portion. The valve membrane includes a first region and a second lower region wherein the first region is folded over the first linking member for attachment and the second region is adjacent the first region and unattached to the first linking member. The second region is movable between a first position to enable
5 blood flow and a second position to inhibit blood flow.

The device preferably further includes a third region folded over for attachment to the first linking member, wherein the second region is positioned between the first and third region.

In one embodiment, the first linking member is curved and traverses a longitudinal
10 axis of the device. In some embodiments, the support is formed at least in part from a shape memory alloy material and the valve membrane is formed at least in part from ePTFE. Preferably, the valve membrane is coated at least in part with an anti-clotting agent. The support can be integrally formed from a laser cut tube.

The device may further include a second linking member, wherein the valve
15 membrane has a fourth region folded over the second linking member for attachment.

In some embodiments, the upper portion of the valve membrane is attached to a bottom region of the first support portion and the lower portion of the membrane is attached to a top region of the second support portion, wherein a section of the lower portion of the membrane is wrapped around a section of the top region of the support
20 portion.

The present invention also provides an implantable device for regulating blood flow through a blood vessel comprising an elongated support dimensioned and configured to be implanted in a blood vessel and a valve membrane supported by the support and

including first, second and third portions. The first portion is attached at a first region of the support, the third portion is attached at a second region of the support, and the second portion is positioned between the first and third portions and unattached to the support. The second portion is movable with respect to the support between a first position to enable
5 blood flow and a second position closer to the support to inhibit blood flow.

Preferably, the first and third portions of the valve membrane form a flap wrapped around a portion of the support, and the second portion forms a flap movable with respect to the first and third portions to create an opening for antegrade blood flow. In a preferred embodiment, the second portion of the valve membrane is closer to a top region than a
10 bottom region of the valve membrane.

The valve membrane may further comprise a fourth portion separate from the second portion and unattached to the support, the fourth portion movable with respect to the support between a first position to enable blood flow and a second position to inhibit blood flow.

15 In one embodiment, the support includes first and second linking members extending between first and second annular portions of the support, and the second portion forms a first flap adjacent the first linking member and the fourth portion forms a second flap adjacent the second linking member, the flaps each creating a space between the flap and the respective linking member during antegrade blood flow to enable blood flow
20 through the space and the flap closing the space during retrograde blood flow.

The present invention also provides an implantable device for regulating blood flow through a blood vessel comprising an elongated support dimensioned and configured to be implanted in a blood vessel and engagable with a blood vessel wall and a valve

membrane. The support includes axially spaced apart first and second support portions and a first linking member linking the axially spaced apart portions to one another. The valve membrane is attached to the linking member, the valve membrane having an upper portion attached to a first section of the support and a lower portion attached to a second section of
5 the support. The valve membrane has an enabling condition to enable blood flow when blood flows in one direction and an inhibiting condition to inhibit blood flow when blood flows in an opposite direction. The upper attached portion of the membrane and the lower attached portion of the membrane remain substantially fixed in position in both the enabling condition and the inhibiting condition and the lower and upper attached portions
10 remain adjacent opposing regions of the vessel wall in both conditions.

The valve membrane preferably includes an intermediate portion between the upper and lower attached portions and a first flap in the intermediate portion, the first flap unattached to the support and movable for creating the flow inhibiting and flow enabling conditions while the upper and lower attached portions remain fixed.

15 The present invention also provides an implantable device for regulating blood flow through a blood vessel comprising an elongated support dimensioned and configured to be implanted in a blood vessel and a valve membrane supported by the support and having a first condition to enable blood flow and a second condition to inhibit blood flow. The valve membrane is positioned in the vessel at a first angle extending across the vessel
20 to traverse a longitudinal axis of the vessel such that opposite ends of the membrane are adjacent opposing walls of the vessel, and the membrane remains substantially at the first angle in the first and second conditions.

Preferably the valve membrane has a first region unattached to the support formed by at least one cut in the membrane and creating an opening adjacent the support during antegrade blood flow. Preferably, the first unattached region moves adjacent the support to close the opening during retrograde blood flow.

5 In a preferred embodiment, the valve membrane has a second region unattached to the support and spaced from the first region, the second unattached region formed by at least one cut in the membrane and creating an opening adjacent the support during antegrade blood flow. In this embodiment, the second unattached region moves adjacent the support to close the opening during retrograde blood flow.

10 In one embodiment, the valve membrane has an upper region and a lower region, and the first unattached region and second unattached region are closer to the top region than the bottom region.

BRIEF DESCRIPTION OF THE DRAWINGS

15 So that those skilled in the art to which the subject invention appertains will readily understand how to make and use the apparatus of subject invention without undue experimentation, preferred embodiments thereof will be described in detail hereinbelow with reference to certain figures, wherein:

Figure 1 is a perspective view of the flow regulating device of the present invention,
20 prior to full assembly;

Figure 2 is a perspective view of the support of the flow-regulating device of Figure 1;

Figure 3 is a side perspective view of the flow regulating device illustrating how the membrane is attached to the frame;

Figure 4 is a front perspective view of the top (distal) portion of the flow regulating device of Figure 1 showing the membrane in the closed position;

5 Figure 5A is a side perspective view showing the membrane in the open position;

Figure 5B is a side perspective view similar to Figure 5A showing the membrane in the closed position;

Figure 6A is a cross-sectional view of the identified area of Figure 5A showing the membrane in the open position, resulting from antegrade blood flow;

10 Figure 6B is a cross-sectional view of the identified area of Figure 6A showing the membrane in the closed position, resulting from retrograde blood flow;

Figure 6C is a top view of the upper region of the membrane of Figure 5B showing the membrane in the closed position;

15 Figure 6D is a top view of the upper region of the membrane of Figure 5A showing the membrane in the open position;

Figure 6E is a top view of the upper region of an alternate embodiment of the membrane shown in the open position;

Figure 7 is a view similar to Figure 4 showing another alternate embodiment of the membrane with flaps forming larger openings for increased antegrade blood flow;

20 Figure 7A is a cross-sectional view similar to Fig 6B except showing the membrane of Figure 7 in the closed position; and

Figure 8 is a drawing of the anatomy of the patient showing two examples of locations of placement of the flow regulating device.

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

Referring now to the drawings wherein like reference numerals identify similar or like components throughout the several views, there is illustrated a flow regulating device
5 constructed in accordance with a preferred embodiment of the subject invention, and designated generally by reference numeral 10. Regulating device 10 includes an elongated support 12 that has upper and lower substantially annular ring portions 14 and 24, each having a series of rounded V-shaped apices 15a facing in an upward direction and a series 15b facing in a downward direction. That is, the upper or distal (with respect to the
10 direction of blood flow) ring portion 14 has a first series of angled struts 13a forming a V and a second series of angled struts 13b forming an inverted V which together form a group of closed substantially diamond shaped cells 19 connected at region 17. Similarly, the lower or proximal (with respect to the direction of blood flow) ring portion 24 has a first series of angled struts 29a and a second series of angled struts 29b, facing in opposite
15 directions and forming closed substantially diamond shaped cells 28 connected at region 27. The cells 28 have upper apices 25 and lower apices 26. For clarity, not all of the identical parts in the drawings are labelled. Note that in the preferred embodiment, the rings and linking member (described below) are preferably integral so that terms “joined”, “connected”, etc. are used for ease of description.

20 Support 12 has two curved linking or connecting members 21a, 21b, best shown in Figure 2 in which the membrane is removed for clarity. The top of each connecting member 21a, 21b extends from a common lower apex 15b of one of the pairs of angled struts 13b of upper ring 14 (see also Figs. 3 and 4) The lower end of connecting members

21a, 21b extend from separate upper apices 25a, 25b, respectively, of cells 28 of lower ring 24. In the illustrated embodiment, the apices 25a, 25b, are about 36 degrees apart as ten cells are formed. However, a different number of cells can be provided with different spacing between apices. Also, it should be appreciated that the connecting members can
5 extend from other apices of lower ring 24 or upper ring 14. The connecting members 21a, 21b have a curve or twist extending close to about 180 degrees (and extending substantially across the vessel when implanted) so that an upper end is connected to one end (viewed radially/transversely) of the device 10 and the lower end is connected to an opposite end (viewed radially/transversely) of the device 10. That is, with ten closed cells
10 in the illustrated embodiment, apex 15b is approximately 162 degrees out of phase from apex 25a and from apex 25b. Other spacing and alternate number of cells is also contemplated.

Although two connecting members are shown, one connecting member or more connecting members could be provided. Also, the connecting members could be spaced
15 further or closer apart and have different curves than shown.

The rings 14, 24 are collapsed to a reduced diameter (profile) position for delivery. The rings 14, 24, when implanted, are substantially perpendicular to the direction of blood flow. Preferably, the rings 14, 16 in their expanded (deployed) configuration are larger in diameter than the internal diameter of the target vessel to apply a sufficient radial force
20 against the vessel to ensure that the device remains in a desired position and orientation after implantation. For example, for use in an 8mm vessel, the rings could have an expanded outer diameter of about 10mm and preferably could be collapsed sufficiently to

be delivered through a 12Fr (4mm) delivery catheter. Others ring diameters are also contemplated.

5 The support 12 is preferably composed of shape memory material, such as NitinolTM or ElgiloyTM, with a shape memorized larger diameter configuration as shown in the drawings. In the illustrated embodiment, the support is laser cut from a tube so that the connecting members and rings are integral. However, it is also contemplated that alternatively the support can be formed from wire(s). Also, it should be appreciated that instead of being integral, separate members could be provided, with separate rings
10 joined by separate linking (connecting) members.

Device 10 includes a valve member or membrane 50 that is operatively associated with support 12 for regulating the flow of blood through a vessel by moving between open and closed positions. Membrane 50 is preferably formed from a sheet of ultra thin membrane material such as a ePTFE material or the like. It is envisioned that the
15 membranes disclosed herein could be bonded or otherwise coated with an anti-clotting or anti-coagulant/anti-thrombogenic agent such as HeparinTM and/or an anti-proliferative coating, to retard the body's desire to reject the implant. In a preferred embodiment, the membrane is coated with an anti-thrombogenic agent and the frame is coated with an anti-proliferative agent, such as DexamethasoneTM by way of example.

20 As shown, valve membrane 50 has an upper portion 52, an intermediate portion 62, and a lower portion 72. With reference to Figure 3 which illustrates how the membrane 50 is attached to support 12 in manufacture, the top portion 52 has first and second flaps 54, 56 which are folded down over respective connecting members 21a, 21b and attached to the membrane to secure the upper portion 52 of membrane 50 about the
25 support 12. Figure

3 illustrates flap 56 already folded in the direction of arrow F4 from its unfolded position shown in phantom. Figure 3 also illustrates flap 54 in its unfolded position before movement in the direction of arrow F3 in manufacture to its folded position depicted in phantom. Flaps 57 and 59 at the uppermost region of membrane 50 are wrapped around
5 struts 13b in the direction of arrows F1, F2, respectively.

With continued reference to Figure 3, the intermediate portion 62 of membrane 50 has flaps 64, 66 for connection to linking (connecting) members 21a, 21b, respectively. Flap 64 is shown in a mostly unfolded position to be folded in the direction of arrows F6 to its folded position shown in phantom where it is attached to the membrane 50. Flap 66 is
10 shown in its unfolded position to be folded in the direction of arrows F5 to its folded position depicted in phantom.

Lower portion 72 of membrane 50 has flaps 74 and 76 which are each folded around a separate strut 29a. Arrows F8, F7, respectively, illustrate the direction of the fold.

Cuts in the membrane 50 create an unattached flap 84 between upper attached flap
15 54 and intermediate attached flap 64 and an unattached flap 86 between upper attached flap 56 and intermediate attached flap 66. These unattached flaps 84, 86 are positioned adjacent the respective connecting member 21a, 21b as shown, but create a respective opening 90, 91 for blood flow between the membrane 50 and connecting members 21a, 21b as described below. Note, alternatively, the flaps 84, 86 can extend over the
20 connecting member, as long as it remains unattached and creates a sufficient space from the linking member to create a sufficiently sized opening to allow blood flow therethrough.

Note that Figure 1 shows the membrane 50 with the flaps open, prior to connection in manufacture, to illustrate how it is wrapped around the support 12 and connected to

other portions of the membrane for securement/attachment of the membrane to the support
12. The flaps, after wrapping over/around the region of support 12, can be connected to
the membrane body by welding, adhesive, suturing or other methods. Also, an
intermediary material can be used to facilitate welding, such as polyurethane or
5 polycarbonate/polyurethane impregnated or otherwise combined with the ePTFE material.
It is also contemplated that the membrane can be attached to the support 12 itself by
methods such as by adhesive or use of suture material.

As can be appreciated, the body portion of the membrane 50 extends substantially
if not entirely across the expanse of the vessel in the open position. However, the openings
10 90 and 91 adjacent the unattached flaps 84, 86 provide a sufficient gap for the necessary
amount of blood flow, it being appreciated by applicants that a normally functioning valve
is only open about 35%. In some embodiments, the openings in the membrane created by
the space between flaps 84, 86 and the support create a space gap in the range of about 5%
to about 15% of the diameter of the vessel. In the alternate embodiment depicted in Figure
15 7, larger openings 90' and 91' are formed to allow more antegrade blood flow. In these
large opening embodiments, a space (opening) can be created preferably representing
about 15% to about 45%, and more preferably from about 15% to about 30% of the
diameter of the vessel. (In all other respects the regulating device of Figure 7 is identical to
that of Figure 4 and the corresponding parts are labelled by numerals with a prime
20 designation and therefore are not discussed herein). These percentages are defined in
terms of the diameter of the blood vessel. For example, if a rectangular opening is formed
of dimension of 2mm x 4mm, and is placed in a 10mm vessel, the cross section occupied
by the two openings (about 16mm) would be about 20% of the overall diameter of the

vessel (about 78mm). It should be appreciated that the foregoing ranges and percentages are provided by way of example and other size openings creating a different percentage opening are also contemplated. Also, other shape openings can be provided other than rectangular, including square, semicircular, etc. Figure 6E shows by way of example
5 substantially semicircular openings 90'', 91'' formed by flaps 84'', 86'', respectively.

Movement of the membrane 50 between an open (blood flow enabling) position/condition to allow antegrade blood flow and a closed (blood flow inhibiting position/condition) to essentially block flow are shown in respective Figures 5A and 5B, and shown in more detail in Figures 6A-6D. In the closed position, however, a minimal
10 amount of blood flow is allowed as will be discussed below.

More specifically, and with reference to Figure 5A, blood flowing through the blood vessel V in the downstream direction (antegrade flow) indicated by arrow "D" will act against the valve membrane 50 in such a manner as to push the body portion upwardly as viewed in the drawing, creating a concave belly on the underside. The blood will travel
15 along the concave surface and up the membrane and the blood pressure will force the flaps 84 and 86 upwardly, separating (spreading) them from the respective connecting members 21a, 21b as also shown in Figures 6A and 6D to form an opening or gap.

After the pulsed blood travels in the direction of arrow D1 (Fig. 5A), through the openings (spaces) 90, 91, the blood backs up in the direction of arrow C of Figure 5B.
20 This retrograde blood flow will act against the angled body of the membrane 50, forcing it downwardly as viewed in Figure 5B to form a convexity on its underside. This downward pressure will force flaps 84, 86 downwardly adjacent to the connecting members 21a, 21b, respectively, and against the connecting member as shown for example in Figure 6B and

6C, thus essentially closing the openings 90, 91 to prevent blood flow therethrough. However, a small amount of blood will force its way between the membrane 50 and the vessel wall as depicted by arrow C1 in Figure 5B, thereby reducing stasis or stagnation that could lead to clotting. In embodiments wherein a larger flap is utilized to create a larger opening, such as in the embodiment of Figure 7, the flap 84' (and 86', not shown) in the closed position would lie adjacent the connecting members, and extend underneath the connecting member (e.g. connecting member 21a') to lie against the vessel wall as shown in Figure 7A, thereby inhibiting blood flow.

It should be appreciated that the membrane extends at an angle across the vessel of about 50 to about 70 degrees to help direct the blood flow and continuously wash the membrane body to prevent blood stagnation. (Other angles are also contemplated) More specifically, blood contacting the body portion of the membrane 50 in the open position will be directed upwardly, along the concave surface, thereby washing the membrane body to wash away clots to reduce the likelihood of clotting. In the closed position, blood contacting the membrane body will be directed downwardly along the angled body to wash the opposing side of the membrane to likewise reduce the likelihood of clotting.

As can be appreciated, the membrane 50 remains at substantially the same angle across the blood vessel in the open (flow allowing) and closed (flow inhibiting) positions/conditions. That is, as shown in Figures 5A and 5B, the upper region of the membrane 50 is adjacent one side of the vessel wall in the open (flow allowing) position. The upper region remains adjacent the same wall in the closed (flow inhibiting) position. Similarly, the lower region of the membrane 50 is adjacent an opposite side of the vessel wall, and remains adjacent that wall in both the open and closed positions of Figures 5A,

5B, respectively. Thus, the upper and lower attached regions of the membrane remain in substantially the same position.

One example of the location of placement of the flow regulating device in a patient's leg is shown in Figure 8 with areas A1 and A2 showing possible placement sites of the device, e.g. upstream or downstream of the native valve V.

If composed of shape memory, the device will automatically expand to the position shown either upon release from a delivery member or in response to temperature change. However, if composed of other materials, the device can be designed to automatically expand due to the springiness of the material or can alternatively be implanted in a blood vessel using a balloon catheter (not shown) as described in copending U.S. patent application serial no. 11,801,691. That is, rings 14 and 24 can be moved from a closed position to an expanded position by inflating the balloon or by use of a mechanical expander. Upon expansion, the rings 14 and 24 apply a force against the vessel wall, thereby being retained therein. The balloon or mechanical expander is then deflated and the catheter is removed from the blood vessel so the device can regulate the flow of blood through the vessel in the manner described above.

In the embodiments disclosed herein showing substantially circular rings, it should be understood that the rings can be shaped to have a size larger than the diameter of the vessel and therefore, depending on the size of the vessel, may not assume a circular shape but have an oval shape pressing against the vessel wall toward a circular configuration. While the above description contains many specifics, those specifics should not be construed as limitations on the scope of the disclosure, but merely as exemplifications of

preferred embodiments thereof. Those skilled in the art will envision many other possible variations that are within the scope and spirit of the disclosure.

1. An implantable device for regulating blood flow through a blood vessel, comprising:
 - a) an elongated support dimensioned and configured to be implanted in a blood vessel, the support including axially spaced apart first and second substantially annular support portions and a first linking member linking the axially spaced apart portions to one another; and
 - b) a valve membrane extending between the axially spaced apart support portions and having an upper portion, a lower portion and an intermediate portion, the valve membrane including a first region and a second lower region, the first region folded over the first linking member for attachment and the second region being adjacent the first region and unattached to the first linking member, the second region movable between a first position to enable blood flow and a second position to inhibit blood flow.
2. The device of claim 1, further comprising a third region folded over for attachment to the first linking member, the second region positioned between the first and third region.
3. The implantable device as recited in claim 1, wherein the first linking member is curved and traverses a longitudinal axis of the device.
4. The implantable device as recited in claim 1, wherein the support is formed at least in part from a shape memory alloy material.
5. The implantable device as recited in claim 1, wherein the valve membrane is formed at least in part from ePTFE.
6. The implantable device as recited in claim 1, wherein the valve membrane is coated at least in part with an anti-clotting agent.
7. The implantable device as recited in claim 1, further comprising a second linking member, the valve membrane having a fourth region folded over the second linking member for attachment.

8. The implantable device as recited in claim 1, wherein the upper portion of the valve membrane is attached to a bottom region of the first support portion and the lower portion of the membrane is attached to a top region of the second support portion.

9. The implantable device of claim 8, wherein a section of the lower portion of the membrane is wrapped around a section of the top region of the support portion.

10. The implantable device as recited in claim 1, wherein the support is integrally formed from a laser cut tube.

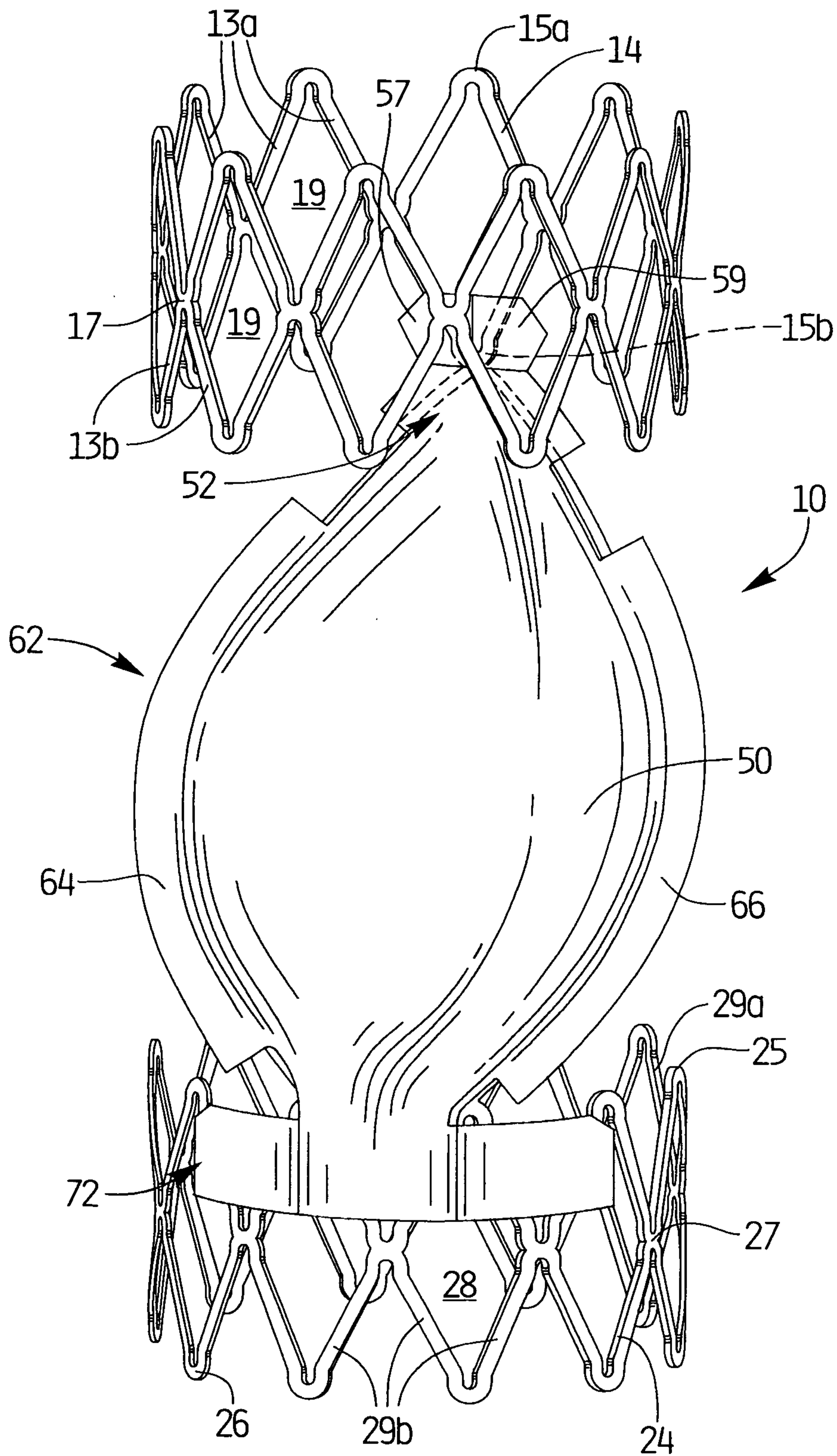


FIG. 1

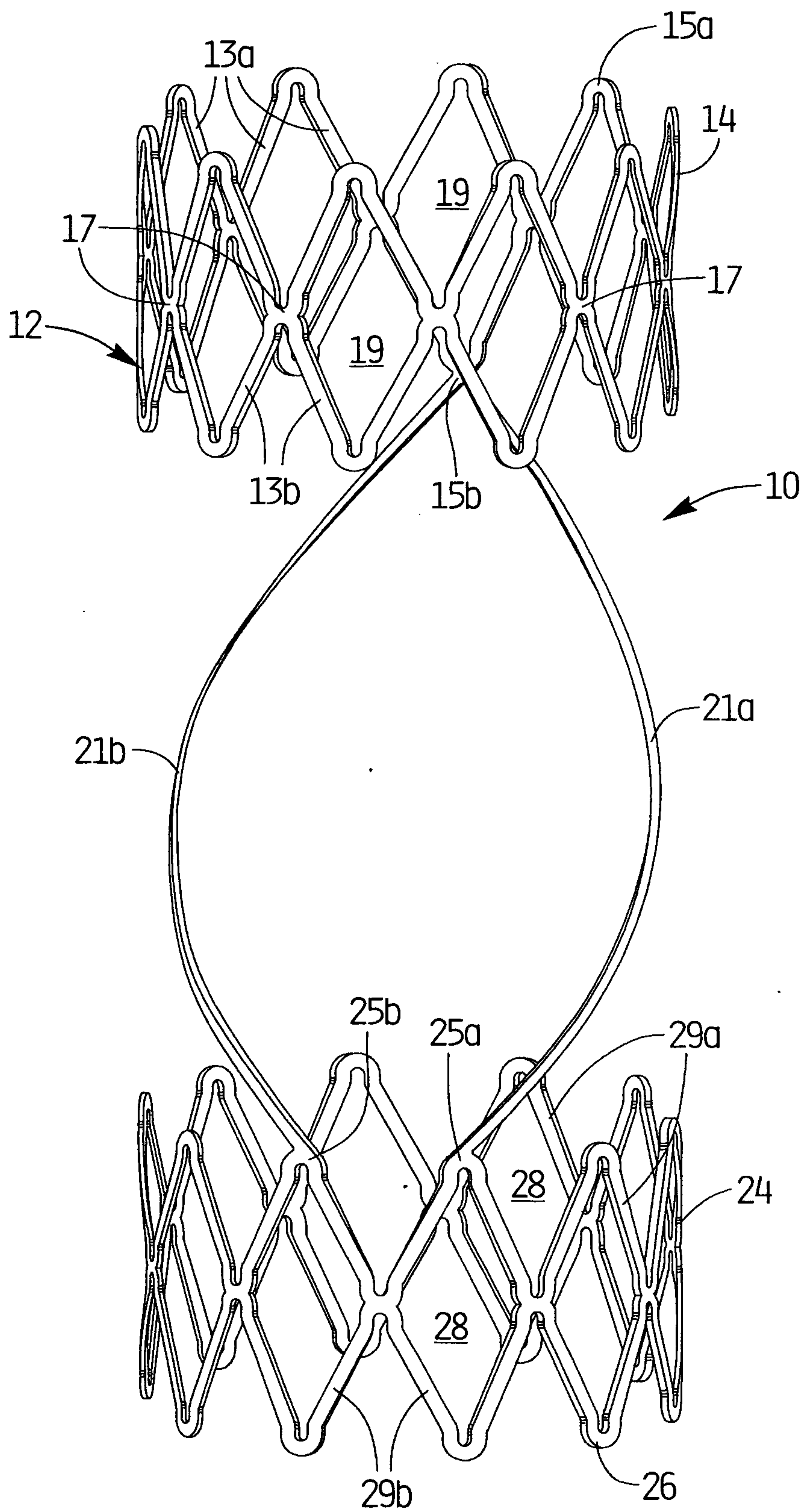


FIG. 2

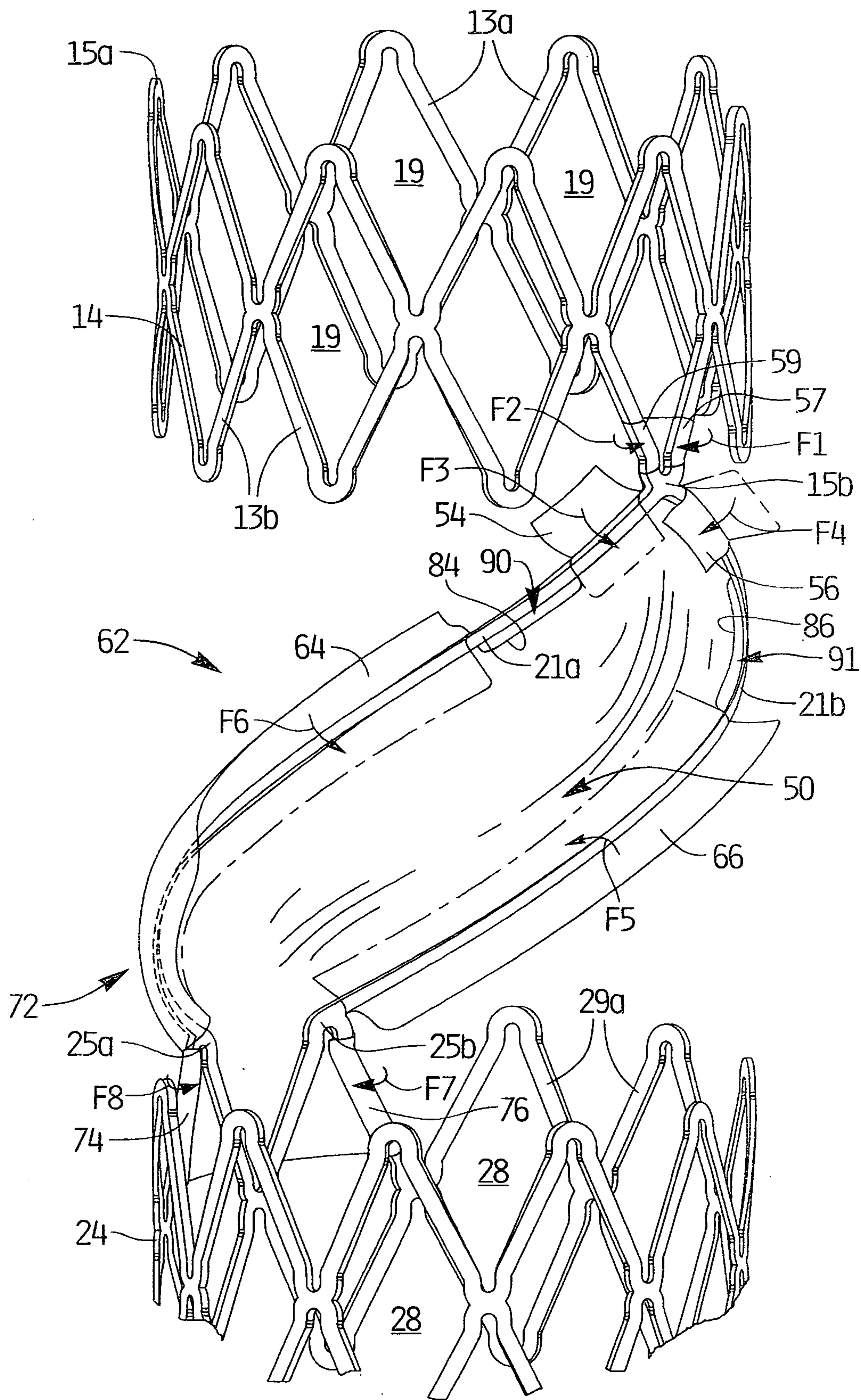


FIG. 3

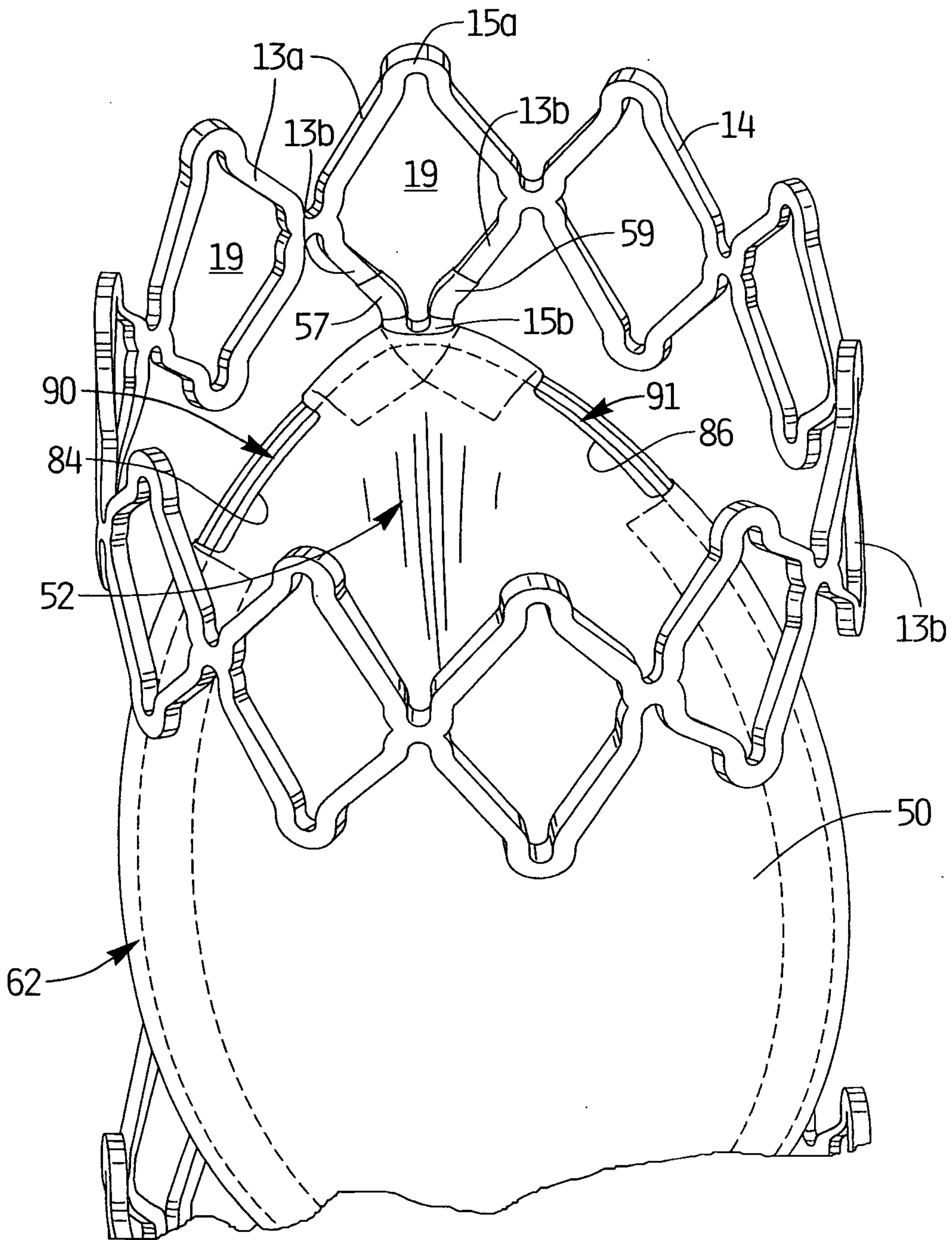


FIG. 4

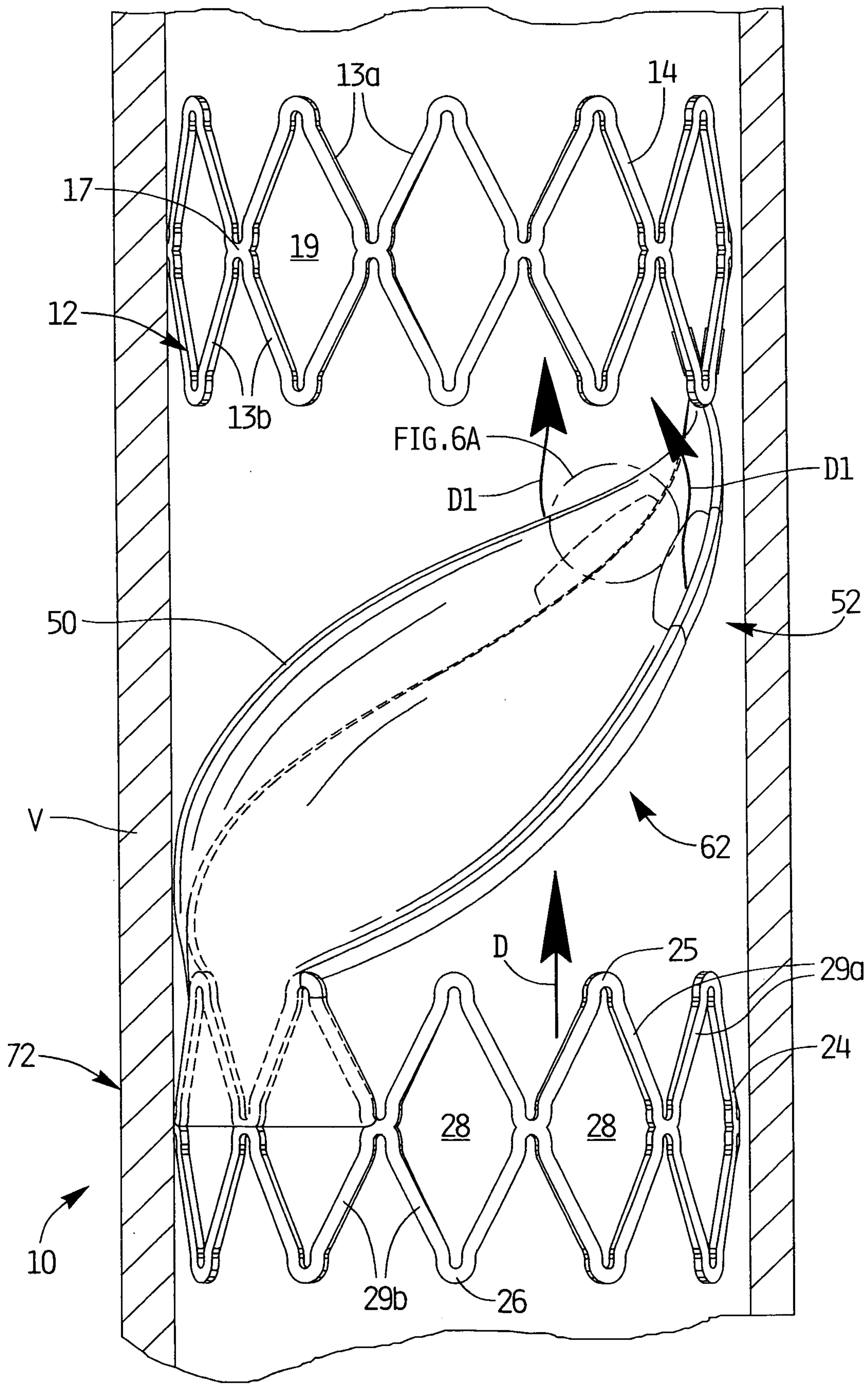


FIG. 5A

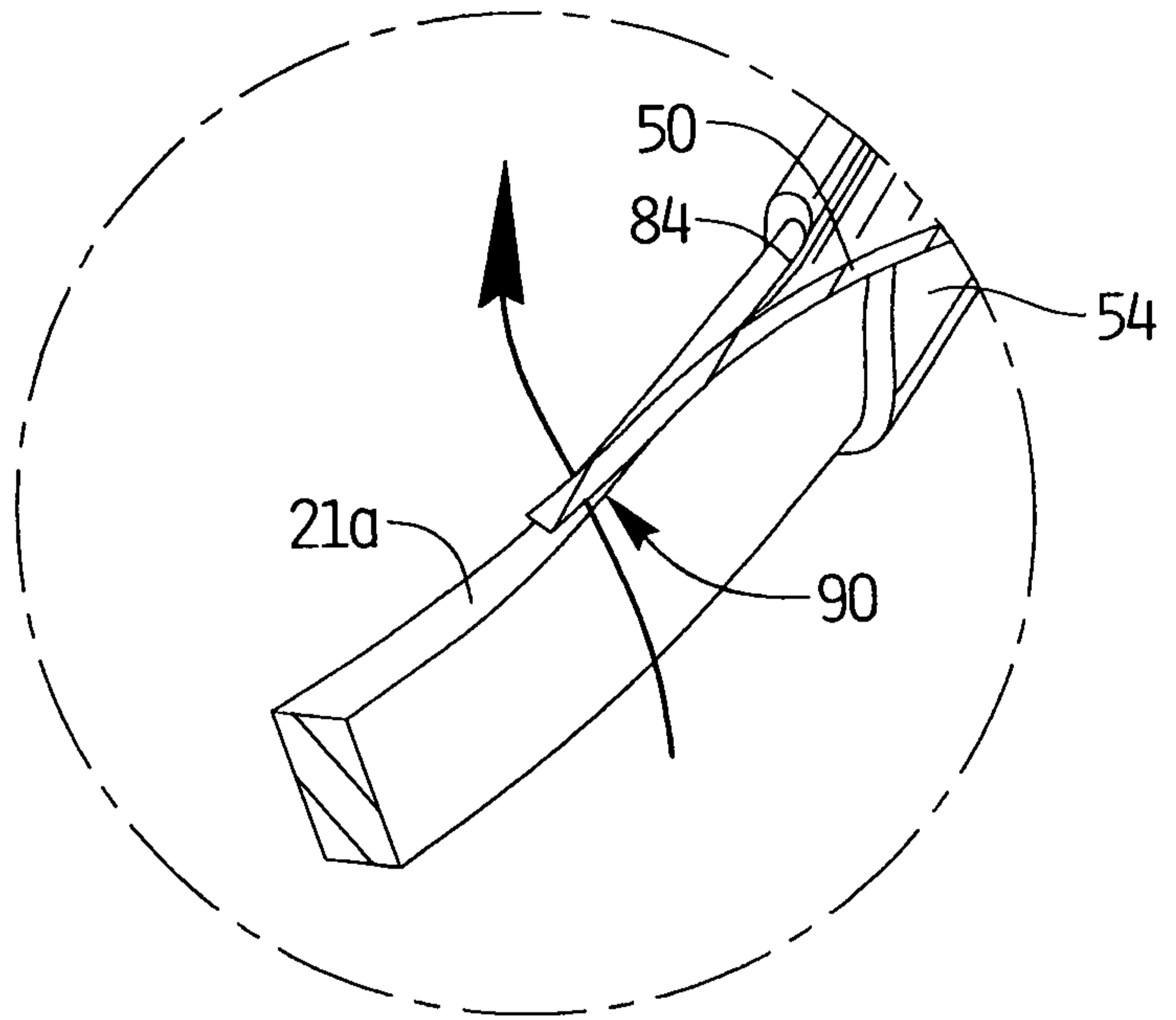


FIG. 6A

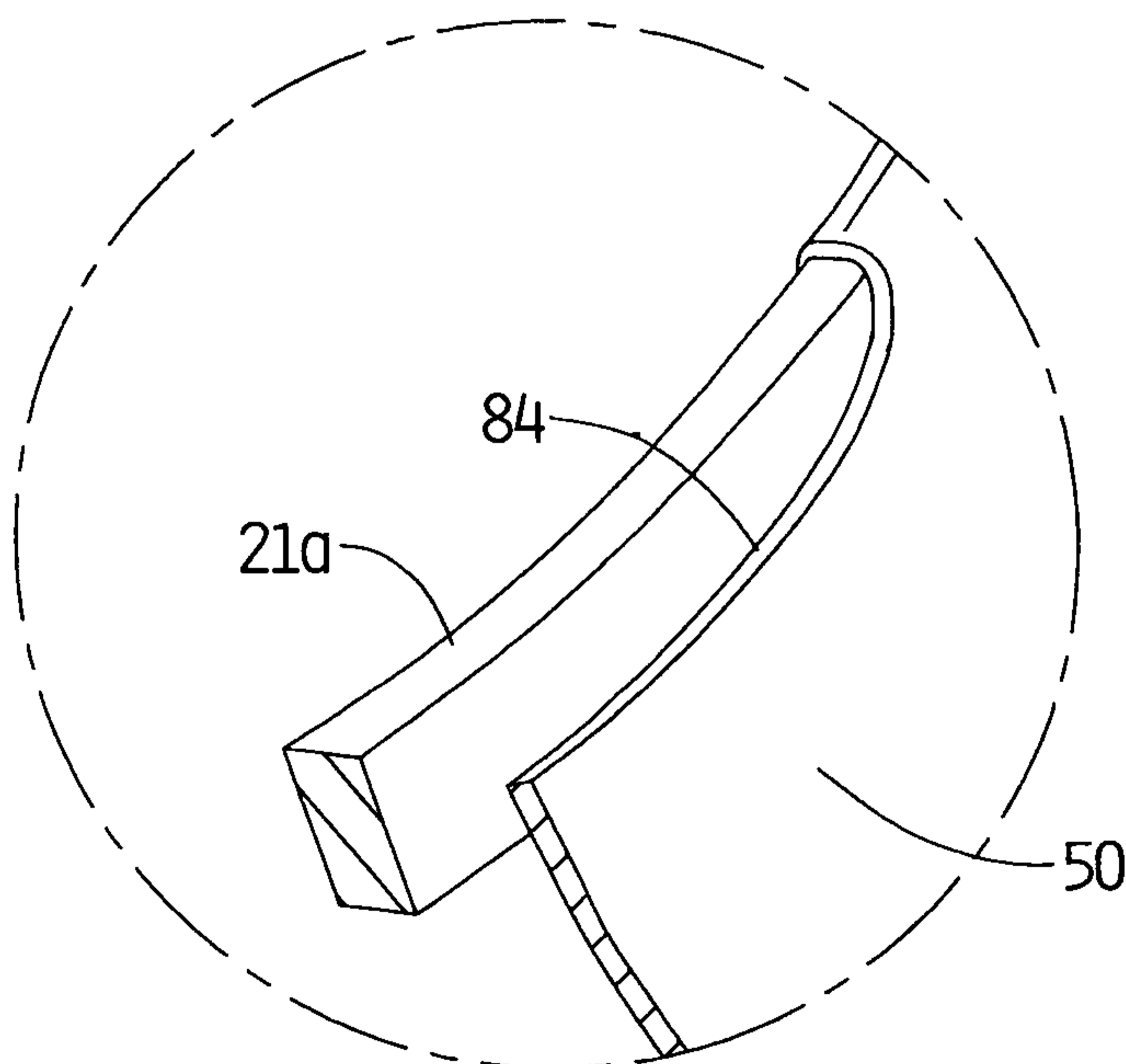


FIG. 6B

FIG. 6C

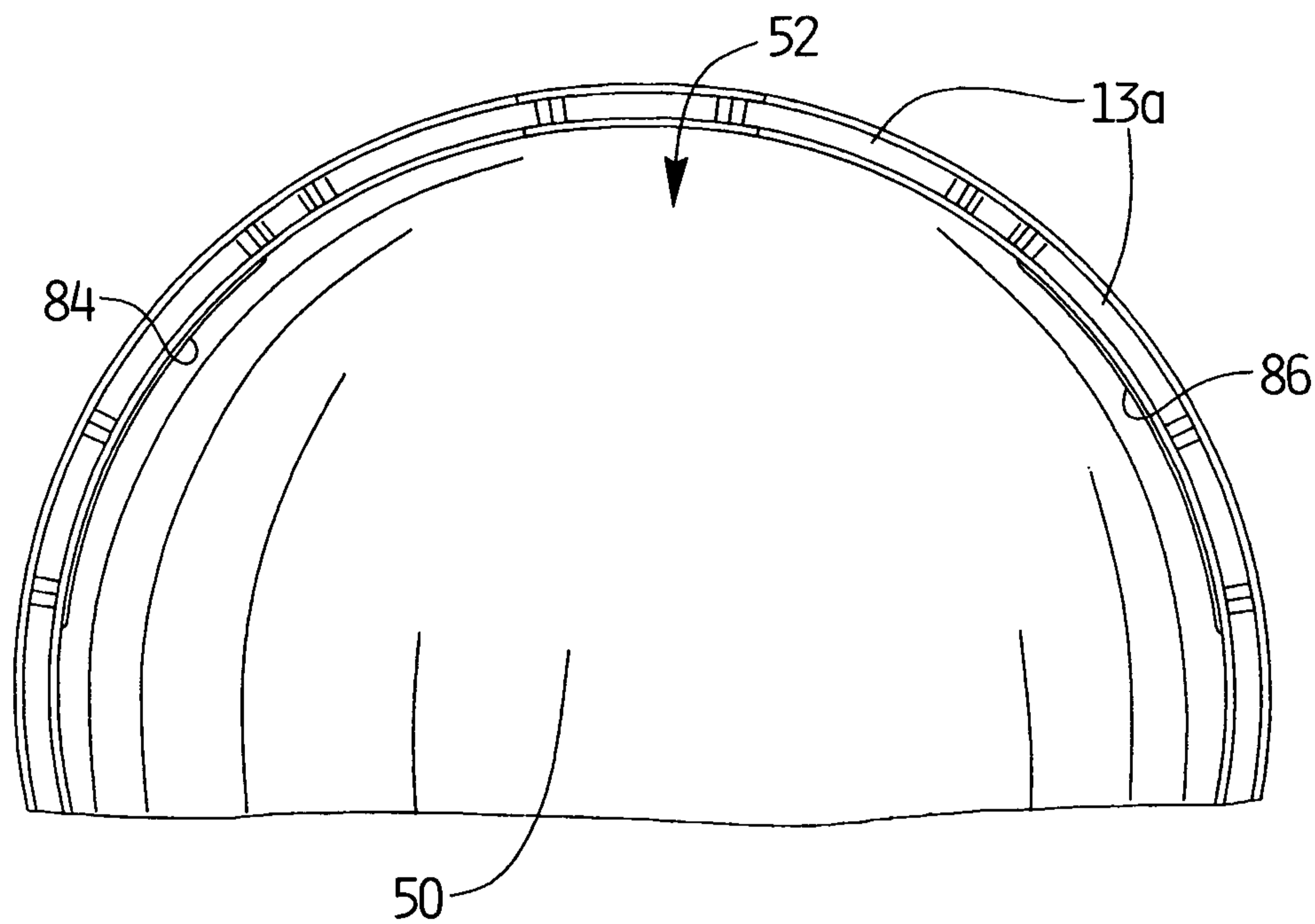
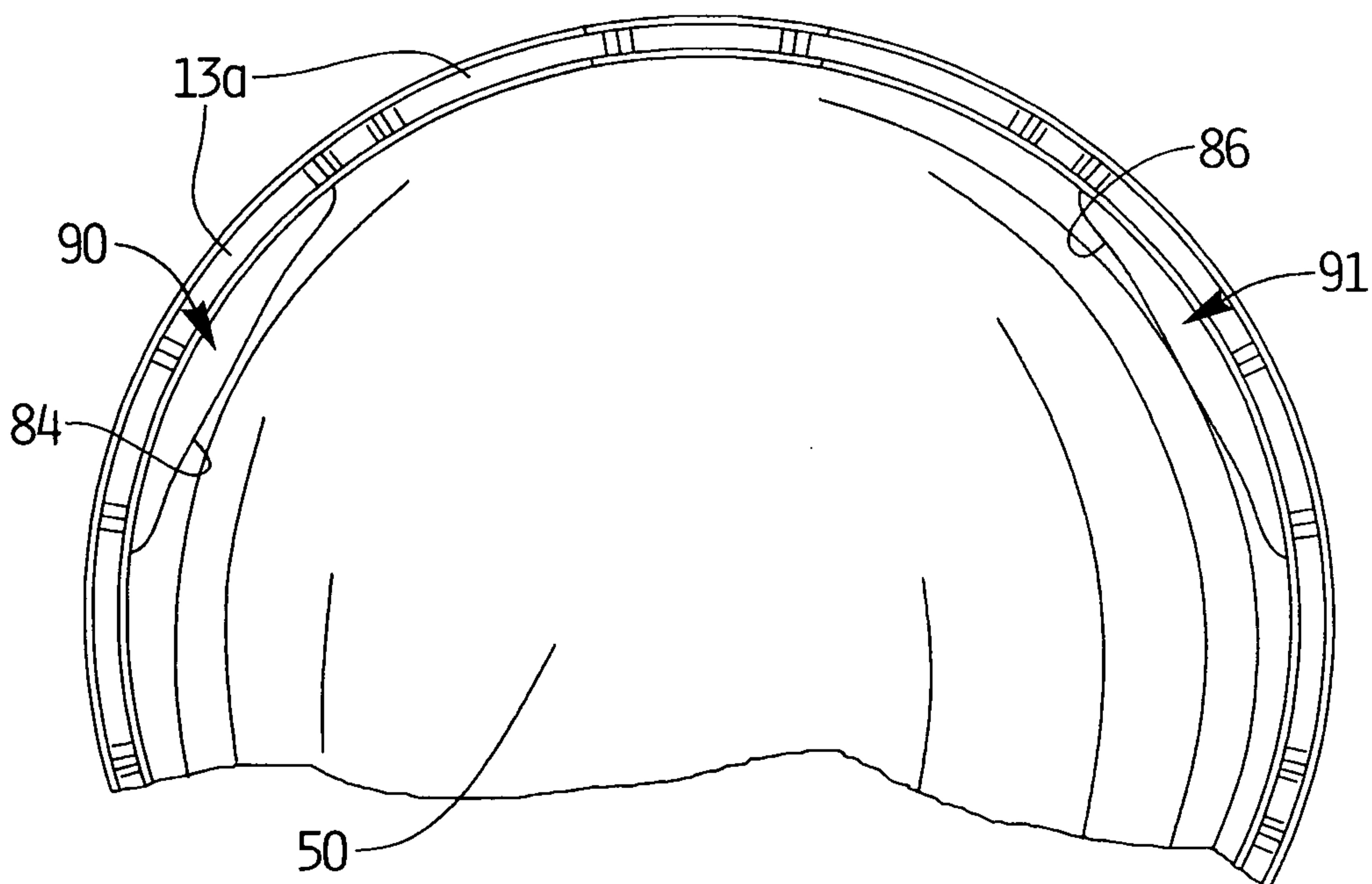


FIG. 6D



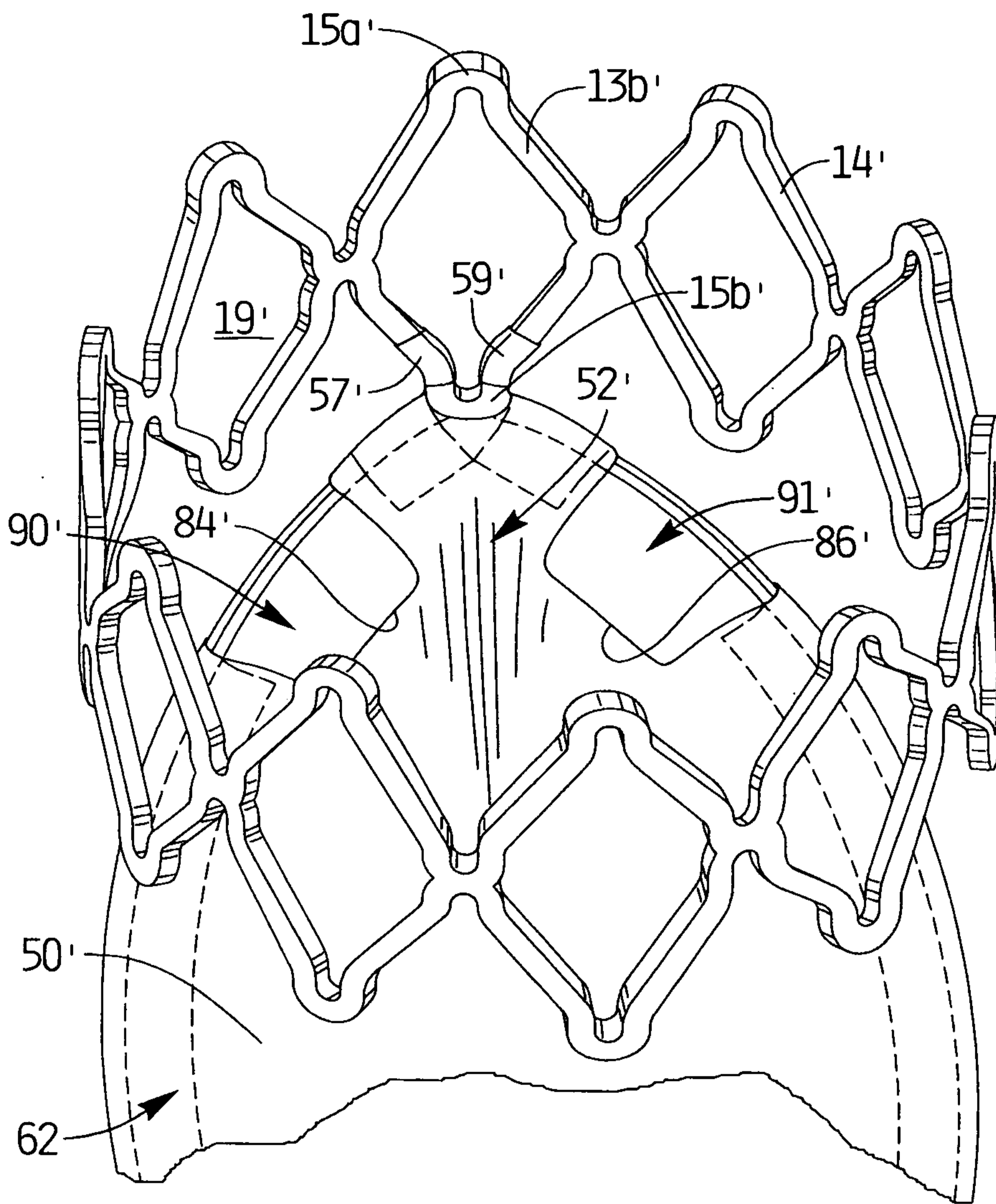
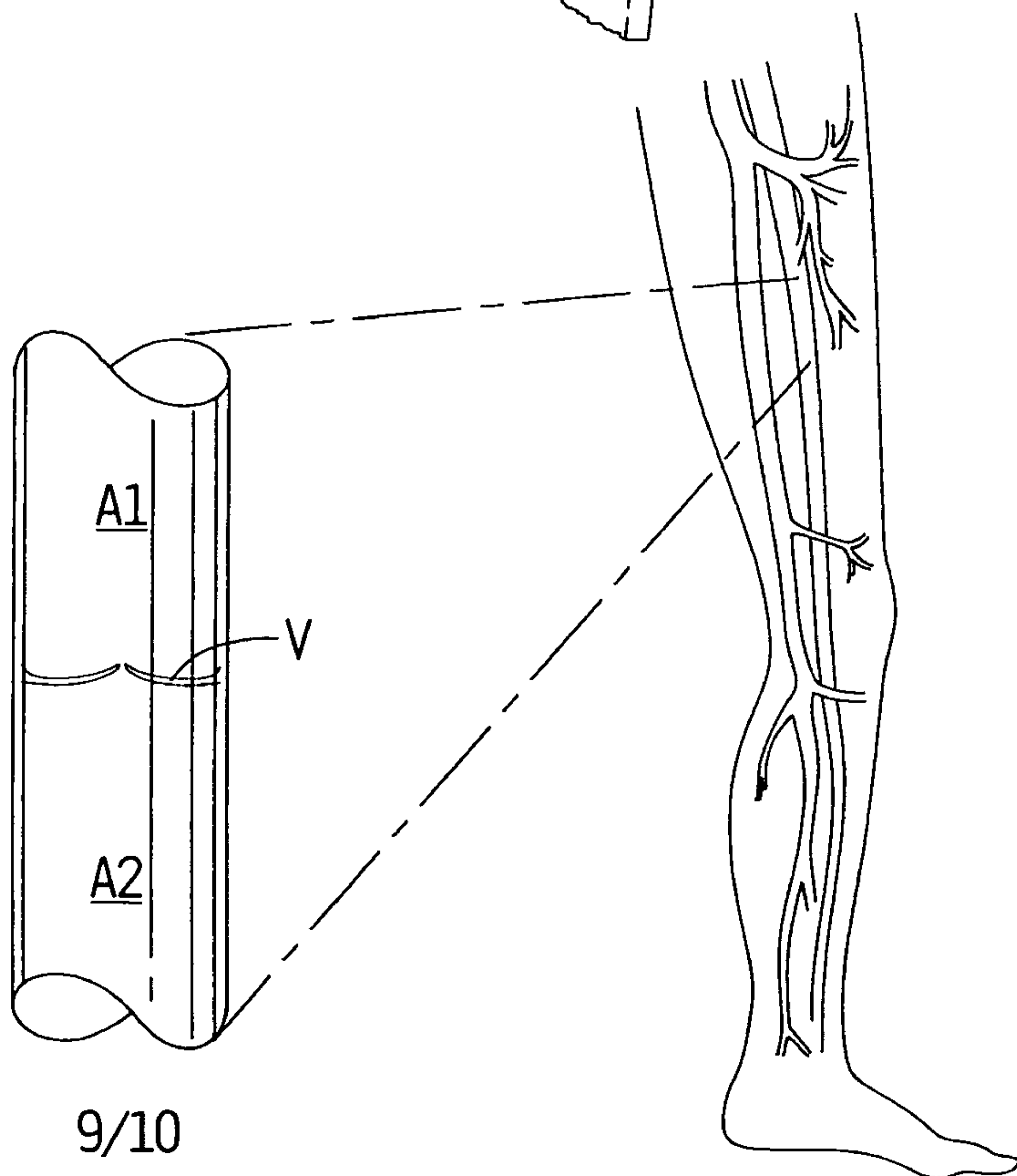


FIG. 7

FIG. 8



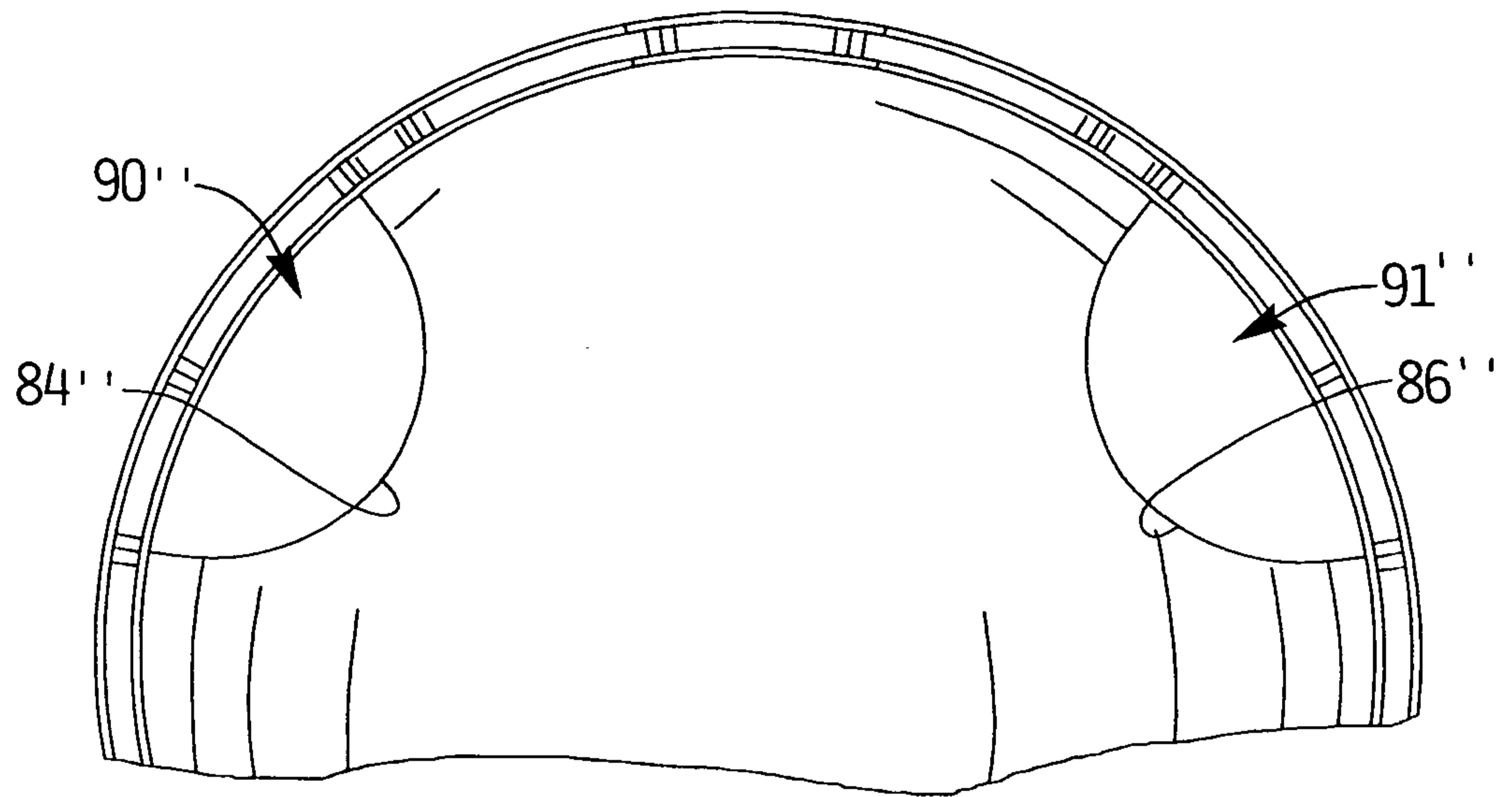


FIG. 6E

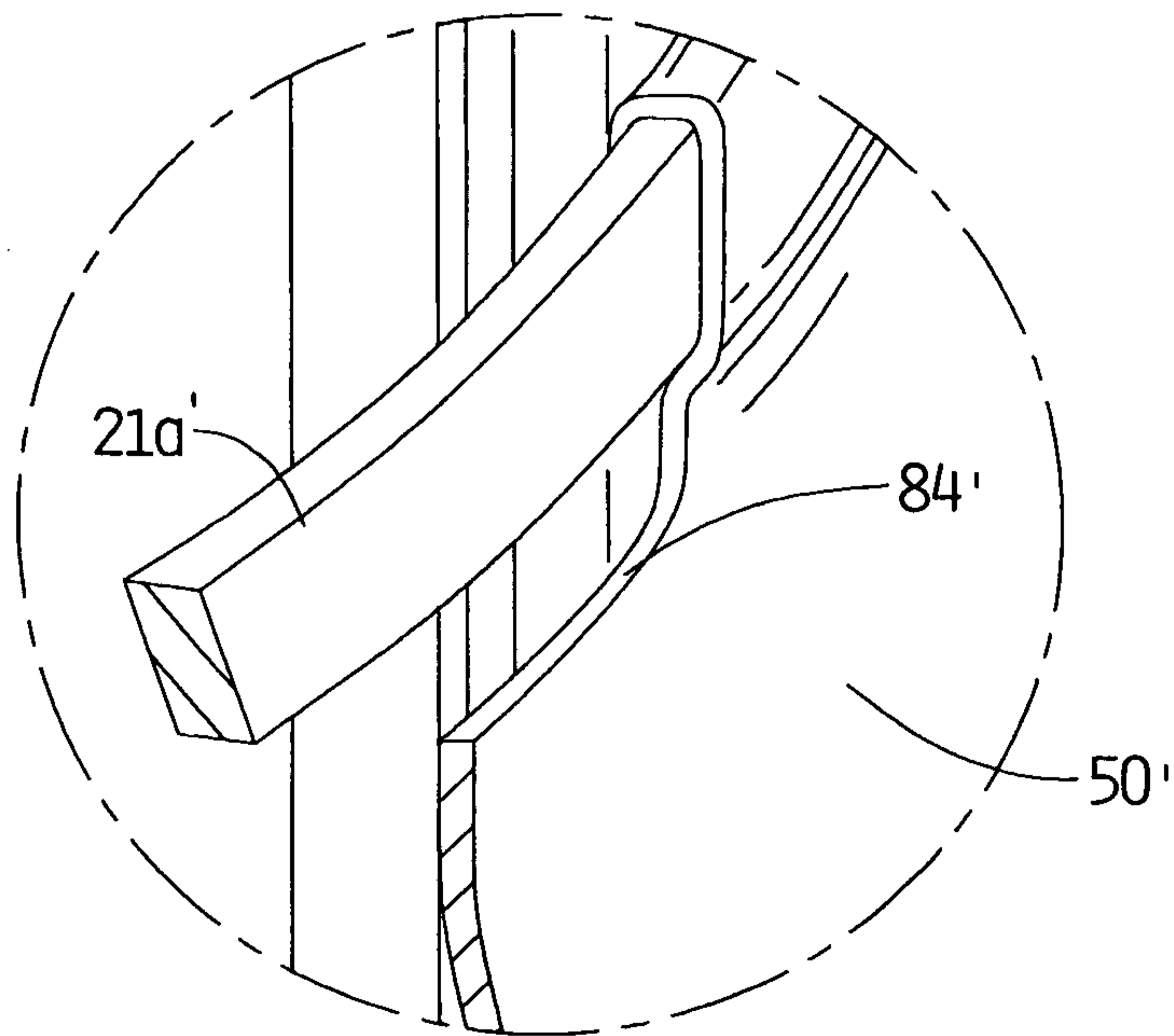


FIG. 7A

