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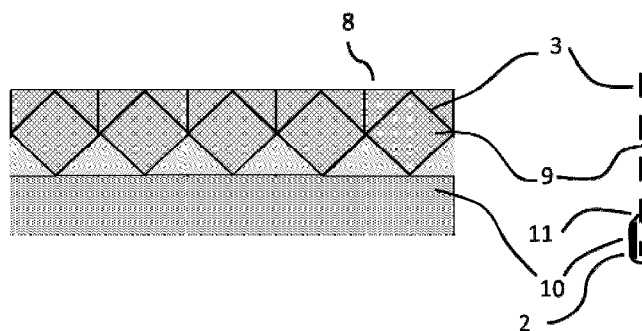


FIG. 2

(57) Abstract: The invention relates to a process for producing a storable and swellable molded body (1) out of bacterial cellulose, this process preparing material that has different swelling behavior. The invention also relates to a molded body produced with the process and a heart valve implant.



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Sealing structure for heart valve implants

The invention relates to a process for producing a storable and swellable molded body made of bacterial cellulose, a molded body made of bacterial cellulose produced according
10 to the inventive process, and a heart valve implant.

US 2013/0331929 A1 describes a sealing system that comprises an additional sealing element at the proximal end of a TAVI valve. This contains a hydrogel that is caused to swell by inflowing fluid. The inflow of fluid is allowed only after implantation by a valve that
15 can be controlled from outside.

US 2013/0018458 describes a system consisting of non-swelling materials (here polyethylene terephthalate, PET) that is designed so that in the inflow area of the TAVI valve overhanging materials of the skirt that is normally sutured inside are fixed to the outside of
20 the stent. This is done in such a way that the overhanging material lies loosely in folds against the outside of the stent in the implanted state. This fold formation in the area of the annulus in turn seals existing leakages.

Sealing by means of swellable hydrogels has negative effects on the durability of these
25 heart valves, since hydrogels generally do not exhibit long-term stability under physiological conditions.

The use of loosely attached PET skirts does not comprise an active element of the seal. Thus, in highly calcified areas of the natural valve annulus leakage flows can still occur,
30 since the PET material cannot conform in a form-fit manner to the calcification.

Starting at this point, the invention has the object of creating a process to produce a storable and swellable molded body that, especially when used for sealing, at least partly reduces the previously mentioned disadvantages, especially leakage flows, that can occur after the implantation of transcatheter heart valves because of so-called paravalvular leaks or leakages.

This object is solved by a process having the features of claim 1 and by a molded body having the features of claim 3, and further by a heart valve implant having the features of claim 4. Preferred embodiments of these aspects of the invention are indicated in the corresponding subordinate claims and are described below.

Accordingly, a process is proposed for producing a storable and swellable molded body of bacterial cellulose, this process comprising at least the following steps:

- i) providing a molded body made of bacterial cellulose;
- ii) Mechanical pressing of parts of the molded body at temperatures in the range of 10°C to 100°C and pressing in the range of 0.01 to 1 MPa for 10-200 min.;
- iii) Treating the pressed molded body with a solution consisting of 20 weight % to 50 weight % glycerol and 50 weight % to 80 weight % of a C1-C3 alcohol/water mixture; and
- iv) Drying the treated molded body.

The inventive process advantageously allows the provision of a swellable, mechanically stable material with very good biocompatibility and hemocompatibility, the material having an area or areas with greatly different swelling behavior. Thus, the process proposed here can provide a material whose swelling behavior can be especially adjusted in desired subareas for special applications. This material is especially preferred for building a skirt (or skirt area) of an artificial heart valve or a heart valve prosthesis, and is preferably simultaneously used as a sealing element in the heart valve's inflow area.

According to the invention, it is preferable to use bacterial cellulose as a biocompatible material. Bacterial cellulose is an extracellular metabolic product formed by microorganisms, so many of its properties are comparable to those of cellulose of plant origin. How-

ever, its purity is significantly higher, since it contains no foreign polymers or other inclusions. The supermolecular structure of bacterial cellulose makes it very hydrophilic and gives it high absorptivity and mechanical strength. For synthesis of cellulose, both gram-negative microorganisms (*Gluconacetobacter* (G.), *Azotobacter*, *Rhizobium*, *Pseudomonas*, *Salmonella*, *Alcaligenes*) and gram-positive ones (*Sarcina ventriculi*) can be used. The most frequently used of these are *G. xylinus*, *G. hansenii*, and *G. pasteurianus*, of which *G. xylinus* is especially important. For this invention, the gram-negative aerobic species *Gluconacetobacter xylinus* (formerly also called *Acetobacter xylinum*) is especially important.

A molded body that is made of bacterial cellulose, especially bacterial cellulose from *Gluconacetobacter xylinus*, and that is treated according to this process is advantageously storable, since drying does not make bacterial cellulose brittle, as is the case with conventional drying processes and many other materials. The cellulose can now be processed and stored in the dry state, without the material's positive properties being lost. Surprisingly, it was possible to show that the material's anti-inflammatory properties and good tolerability by the body are preserved just as well as its high mechanical strength.

First, the bacterial cellulose is prepared, preferably in a form suitable for later use. Thus, for example, layers of bacterial cellulose are precipitated, in a manner known in the art, from glucose-containing nutrient solutions inoculated with *Gluconacetobacter xylinus*, and are air-dried. It is just as conceivable to allow a coating of highly purified cellulose fibers to grow directly on a substrate, for example the metallic base body of a stent.

Using suitable culture vessels, it is possible, e.g., to produce layers of bacterial cellulose with different material thickness. To do this, the culture vessel comprises, e.g., a gas-permeable silicone layer of variable thickness that is in contact with the culture solution to be held by the culture vessel. In areas where the silicone layer is of reduced thickness, more air diffuses to the boundary layer between the culture solution and the silicone layer, with the consequence that aerobic bacterial growth increases in this area so that more cellulose is deposited there. In this way it is possible, for example, to produce layers of bacterial cellulose whose thickness ranges from 2 to 10 mm. Thus it is possible to make available a suitable implantation material that can have a thickness greater than that of naturally occur-

ring tissues of human or animal origin which are suitable for the preferred applications as heart valve prosthesis material.

Preparing the necessary molded body from bacterial cellulose might require other preparatory measures, such as purification, pressing, predrying, and cutting and trimming the material. The second step of the inventive process involves subjecting the molded body made of bacterial cellulose required for the respective application to a hot pressing step. The primary goal of the hot pressing step is to remove all or most of the water. To achieve this goal, it is advantageous if this pressing is done sufficiently long and under suitable pressure conditions. The pressure should not be selected to be so strong that the material is mechanically damaged or suffers destruction in the form of cutting or crushing.

Preferably the entire molded body or parts of the molded body are mechanically pressed in the second step at temperatures in the range of 10°C to 100°C and pressed in the range of 0.0005 to 1.5 MPa, more preferably 0.01 to 1 MPa for 10-200 min. Hereby the swelling capacity of the cellulose is reduced and can thus be adjusted to meet desired requirements. Also the mechanical stability of the material is increased.

In the third step, the pressed molded body is preferably treated with the C1-C3 alcohol/water mixture (for example methanol, ethanol, 1-propanol, and 2-propanol) and glycerol, especially a glycerol-containing isopropanol/water solution, this treatment especially being washing or incubation in the solution.

The solution preferably contains between 20 weight % and 50 weight % of glycerol, the rest being the C1-C3 alcohol/water mixture.

The ratio of C1-C3 alcohol to water in the C1-C3 alcohol/water mixture is preferably between 90 to 10 and 70 to 30. Especially preferred is a C1-C3 alcohol/water mixture formed of 80 weight % C1-C3 alcohol, especially isopropanol, and 20 weight % water.

It is preferable for the proportion of water in the incubation solution consisting of glycerol and a C1-C3 alcohol/water mixture not to exceed 20 weight %.

The solution can contain other components, however it is preferably limited to the mentioned three components. Usually, the time period of the incubation in the solution is, e.g., 0.5 to 24 h, however preferably 12 hours.

5 Then, the molded body treated with the solution is preferably dried. This can be done by suitable processes. In one embodiment, the drying can be done in the air (1 to 2 days). Air drying at room temperature (typically between 20 and 25°C) removes the alcohol that is present and most of the water from the cellulose. The drying can also be done under vacuum or in a climate-controlled cabinet. After drying, the cellulose regularly still has a glycerol content between 0.1 and 10 weight %, with a reference value of 1.5 weight %. The
10 presence of water cannot be excluded, since glycerol is hygroscopic.

An especially preferred embodiment of the inventive process provides that in the second step ii) of the process the temperature is preferably in the range from 80°C to 100°C and
15 the pressure is preferably in the range from 1.5 MPa to 2 MPa. In a different embodiment the pressure can be preferably in the range from 1.0 to 10 kPa and more preferably 1.5 kPa to 2 kPa at a temperature range of 80°C to 100°C.

The bacterial cellulose treated according to the inventive process is advantageously storable,
20 ble, the desired anti-inflammatory properties and compatibility of the material being preserved.

It has proved advantageous that the inventive process can also be used to change the swelling capacity of the cellulose in a selective manner. Here the invention is based especially
25 on the knowledge that dried bacterial cellulose, especially bacterial cellulose of *Gluconacetobacter xylinus*, can, contrary to prevailing opinion, be completely or almost completely rehydrated using the present process or rather special drying process, or the water absorbency can be even further increased by the drying process in parts or portions, while the second step ii) can specially limit the swelling behavior of other subareas, thus allowing
30 the water absorbency to be adjusted.

Therefore, the swelling capacity of the entire molded body or parts of the molded body can be adjusted by the mechanical pressing in step ii) to meet the existing requirements for the respective application. In other words, the swelling capacity of different areas of one and the same molded body can vary independently of one another.

5 Accordingly, another aspect of the invention relates to a storable and possibly swellable molded body made of bacterial cellulose as described in claim 3 that was produced by the previously portrayed inventive process.

10 In the context of the invention, a molded body is understood to be any sort of a physical piece molded in any way. In the simplest case, this can be a flat-shaped body perceived to be two-dimensional (with relatively small thickness compared with its width and length) or an almost two-dimensional planar piece (similar to a strip of fabric). In the same way it is understood to mean more complicated three-dimensional shapes such as cylindrical tube sections, all the way to more complex shapes such as, for example, heart valves.

15 Another aspect of the invention relates to a heart valve implant comprising a supporting stent, a heart valve element, and a skirt, the skirt having at least one inventive molded body, or comprising one, or being formed of at least one molded body (1).

20 A preferred embodiment of the inventive heart valve implant provides that the at least one molded body has at least one area that has lower swelling capacity than an adjacent area of the molded body, preferably due to treatment with the mechanical pressing described in step ii). It is also conceivable to lower the swelling capacity of the entire molded body defined by the aforementioned pressing.

25 A preferred embodiment of the inventive heart valve implant also provides that the skirt comprises an area for sealing paravalvular leakages. Here paravalvular leakages mean leakages in which blood flows past the implant, between the surrounding vessel wall or the native heart valve and the implant.

30 A preferred embodiment of the inventive heart valve implant also provides that the skirt is attached in the luminal and/or abluminal area of the supporting stent. Here the luminal area

of the supporting stent comprises, in particular, an inner surface of the stent, while the abluminal area of the supporting stent comprises an outer surface of the supporting stent facing away from this inner surface. This skirt can have areas or subareas that do not consist of bacterial cellulose as described here, but rather of other materials. However it is just as conceivable for the skirt to consist of bacterial cellulose as described herein. In an embodiment in which areas of the skirt consist of materials other than bacterial cellulose as described here, then the skirt comprises at least one molded part made of bacterial cellulose as described herein that has been treated according to the process proposed here.

A preferred embodiment of the inventive heart valve implant also provides that the skirt runs in the luminal and abluminal area of the supporting stent and furthermore that the skirt has reduced swelling capacity in the luminal area, preferably due to treatment by the mechanical pressing described in step ii), at least parts of the skirt furthermore having a higher swelling capacity in the abluminal area.

A preferred embodiment of the inventive heart valve implant also provides that the skirt is attached on the luminal side of the supporting stent and that at least one molded body, preferably multiple molded bodies, are attached, preferably sutured in, between the stent struts and the skirt attached on the luminal side. This at least one molded body is made of the bacterial cellulose proposed here, and has areas with increased swelling behavior. The at least one molded body or multiple molded bodies that have increased swelling behavior is/are preferably arranged between the supporting stent and a skirt made of non-swella-
ble material, the increase in volume of the swelling molded body being directed radially outward, causing swelling between the stent struts. This skirt running in the luminal area can be made of bacterial cellulose as described here or also of other suitable, especially non-swella-
ble materials such as polymers or other artificial materials or biological tissue, especially of animal origin, such as pericardium or lung, stomach, or intestinal tissue. In a preferred embodiment, the at least one molded body is attached between a node of the stent framework and the skirt running in the luminal area. In another embodiment, the multiple molded bodies are arranged in such a way that molded parts attached next to one another border one another so as to form preferably at least one closed ring in the peripheral direction of the skirt. Embodiments involving luminal arrangement in the stent framework have

the advantage, in addition to effective sealing of leakages, that complication-free re-sheathing is possible with them.

5 A preferred embodiment of the inventive heart valve implant also provides that the skirt is attached in the luminal area to an end of the supporting stent close to the heart valve or in the inflow area, and that the molded parts form at least two closed rings in the longitudinal direction. It is advantageous for the at least one molded body to be sutured between the skirt and the stent framework, preferably to the stent struts and also to the nodes of the stent framework.

10 A preferred embodiment of the inventive heart valve implant also provides that at least some of the borders or edges of the aforementioned molded body run on the stent struts of the supporting stent.

15 A preferred embodiment of the inventive heart valve implant also provides that the skirt is attached in the luminal area of the supporting stent and that the areas that run under the stent struts of the supporting stent have reduced swelling capacity, preferably due to treatment with the mechanical pressing described in step ii).

20 A preferred embodiment of the inventive heart valve implant also provides that the skirt runs in the luminal and abluminal area of the supporting stent and is alternately braided around the stent struts of the supporting stent in the form of at least one band running around the circumference, and that the areas that run on the luminal side under the stent struts of the supporting stent have reduced swelling capacity, preferably due to treatment
25 with the mechanical pressing described in step ii).

A preferred embodiment of the inventive heart valve implant also provides that the heart valve element has at least one heart valve leaflet made of an inventive molded body.

30 A preferred embodiment of the inventive heart valve implant also provides that the heart valve element has three heart valve leaflets made of one inventive molded body, or each made of one inventive molded body.

Further features and advantages of the invention should be explained below by the description of sample embodiments, especially on the basis of the figures. The figures show

- 5 Fig. 1 (a) On the left, a top view of inventive molded bodies for use as sealing elements to prevent paravalvular leakages when there is a heart valve implant. On the right, in the plane of the section along the stent axis, the molded bodies 1 form a ring; (b) The same views as under (a) with the difference that the molded bodies 1 form two rings; and
- 10 Fig. 2 a skirt suitable for a balloon-expandable stent framework. On the left in unrolled top view. On the right in the section plane along the stent axis.
- 15 Fig. 3 a skirt suitable for a balloon-expandable stent framework. On the left in top view after the skirt is folded down. On the right, top view after skirt parts have been cut away at the lower end of the prosthesis.
- 20 Fig. 4 a simplified representation of the stent framework with stent struts and nodes.
- 25 Fig. 5 a view of the skirt area, in which strips of cellulose run above and below the stent struts.
- 30 Fig. 6 another view of the skirt area, in which strips of cellulose run above and below the stent struts.
- 30 Fig. 7 a skirt for a balloon-expandable stent framework. On the left, a piece of cellulose is shown in which lattice-shaped areas have been made with reduced swelling capacity. On the right, the piece of cellulose that is shown alone on the left with a matching stent framework having dimensions such that the stent struts come to lie over the areas with reduced swelling behavior.

Example 1

Native microbial cellulose is incubated overnight in a 20-30 weight % alcoholic glycerol solution (e.g., 30 weight % glycerol, 56 weight % isopropanol, 14 weight % water) and then air-dried at room temperature. Using a cutting device, small pieces 1 of swellable cellulose are separated, as shown in Figure 1, and sutured between the stent struts 3a, 3b, 3c, 3d and the skirt area (skirt) 6 running around supporting stent 3 in the peripheral direction U. The individual stent struts 3a, 3b, 3c, 3d are arranged in such a way that every four such adjacent struts 3a, 3b, 3c, 3d of the supporting stent 3 delimit an opening, in particular a rhombus-shaped one, that is also called rhombus for short. Every four of these struts 3a, 3b, 3c, 3d are always connected with one another through a node 4, in particular they are formed to one another in one piece. An upper or lower half of such a rhombus is called an upper or lower semi-rhombus.

The suture points 5 are attached in the nodes 4 of the rhombi, which are in the lower third of supporting stent 3. One element 1 is attached to each node 4 of the lowermost rhombus plane so that this element 1 is fixed between node 4 and skirt 6. This element 1 has, in the area of the node, reduced swelling capability introduced by the process presented herein produces by means of hot pressing, and in all other areas this element 1 has increased swelling capability. Figures 1a and 1b show two embodiments regarding this in which the elements 1 are attached to nodes 5 so that the elements 1 come to lie against one another. If sufficiently many elements 1 are fastened to the supporting stent 3, the elements 1 form a ring running around the stent framework (Fig. 1a), or even two rings, as shown in Figure 1b.

Example 2

Microbial cellulose (here also called bacterial cellulose, in the example shown herein with a thickness of around 6 mm) is partially dried using a hot press, which reduces the thickness of the dried area by a factor of 50 in comparison with the undried area. After partial drying, the microbial cellulose is incubated overnight in a 20-30 weight % alcoholic glycerol solution (e.g., 30 weight % glycerol, 56 weight % isopropanol, 14 weight % water)

and then air-dried at room temperature. In the non-hot pressed area, the cellulose treated in this way has a layer thickness of 0.5 mm to 0.7 mm and in the hot-pressed area it has a layer thickness of less than 0.1 mm. When remoistened, the layer thickness increases to 4.0 mm to 5 mm in the non-hot pressed area. By contrast, the cellulose in the hot pressed area
5 only swells up to a layer thickness of 0.1 mm to 0.2 mm.

Example 3

Using a cutting device, e.g., correspondingly matching parts are cut out of the non-woven
10 cellulose (1) treated in Example 2 to build a skirt or a skirt area. After that, a skirt can be formed, as shown in the embodiments of Figures 2 und 3. The lower third of it consists of non-hot pressed cellulose 2 that has an increased swelling capability. The non-woven cellulose for the skirt area of a prosthesis is oriented so that the non-hot pressed area comes to lie downward, toward the operator. An operator can be a certified, experienced, and well-
15 trained specialist in the area of suturing heart valve heart valve prostheses. The lower area is folded up once (labeled in Figure 3 by the arrow and F), so that the lowermost cell row of the inflow area is double covered. Then, the three skirt parts are cut out of the cellulose, the gaps between the struts not being cut out in the inflow area. The folded part is sutured to the skirt, preferably using Armenian suturing technique, to prevent the possibility that
20 blood will sneak through. After that, three skirt parts with 3 leaflets are sutured together. Then, the three valve parts are sutured into a complete valve. After the valve inspection, the complete valve is sutured into the stent. Thus, in this embodiment all the valve material, together with the area especially capable of swelling, lies inside the stent. This embodiment is especially advantageous since it is possible to carry out re-sheathing without com-
25 plications. At the end, a small pair of curved scissors is used to trim the gaps between the struts in the inflow area (Fig. 3, left side, bottom).

Example 4

30 Microbial cellulose cut into strips or threads is woven into the stent structure. When this is done, the honeycomb structure of the stent is exploited by always passing the thread/strip once over and once under the strut.

The parts of the thread/strip that lie beneath the strut (between the stent and the inner skirt) can be modified by hot pressing so that they do not swell, or do so only very little. Thus, the inside diameter of the valve does not shrink, or shrinks only very little.

- 5 This processing prevents longitudinal slippage of the resulting structure.

The initial and final thread(s)/strip(s) can either be tied together, and thus form a loop around a strut, or be tied directly to a strut. In both cases a reduction of suture points is achieved, in direct comparison with the flat skirt.

10

Two embodiments are considered in detail as examples of this. Figure 4 first shows, as a starting point, a stent with stent framework 3 and stent struts 3a, 3b, 3c, and 3d, which form a rhombus. At one vertex of the rhombus there is a node 4.

Starting from such a stent, Figure 5 shows an embodiment in which strips of the inventive
15 cellulose are woven into the stent structure. In this embodiment, the strips are woven so that they pass over and under the nodes 4. This produces surfaces 7a that are over stent struts 3a, 3b, 3c, and 3d and nodes 4, and surfaces 7b, that lie under them. As is also shown in Figure 7, this cellulose can be pretreated so that areas that lie under stent struts 3a, 3b, 3c, and 3d and nodes 4 have lower swelling behavior. The cellulose strips can preferably
20 also be arranged so that the edges of the strips overlap on a narrow width, preventing a simple flow (indicated by broken lines).

Figure 6 shows another embodiment in which strips of the inventive cellulose are woven into the stent structure. In this embodiment, the strips do not, as in Figure 5, pass under and over the nodes 4, but rather over and under stent struts lying in a row, preferably directly
25 opposite stent struts 3a and 3c and 3b and 3d in alternation. In Figure 6, stent struts that lie under the cellulose are shown as broken lines, while stent struts that lie above the cellulose are shown as a thick, solid line. Figure 6 also shows areas that lie over the stent structure (7a) and that lie under the stent structure (7b). Interweaving the cellulose into the stent structure produces a steady alternation between areas 7a and 7b.

30

Example 5

A planar piece of microbial cellulose is fastened to the outside of the stent structure. This renders it possible to tell whether the surface is sutured with the stent at a few suspension points, or at many points along the struts (quilt principle).

5 Here it is crucial that the microbial cellulose can be modified by hot pressing in the areas of the sutures so that its swelling characteristics are clearly decreased there. This characteristic can clearly reduce the load on the sutures, without losing the sealing characteristic caused by swelling in the decisive regions radially surrounding the stent body.

10 For further illustration, see the example in Figure 7. Figure 7 first shows, on the left, a piece of cellulose 1 in which lattice-shaped areas with reduced swelling capacity 11 have been made. These areas 11 can be in the area of sutures, but also under sutures and the stent struts, for example, as shown on the right. Here a piece of cellulose is shown, such as is shown alone on the left, with a matching stent framework 3 that has dimensions such
15 that stent struts 3a, 3b, 3c, and 3d and nodes 4 come to lie over the areas with reduced swelling behavior 11, and thus do not exert excessive pressure on the sutures or the stent framework 3, and such that they also contribute to good sealing due to the increased swelling behavior between the stent struts.

20 **Example 6**

For a balloon-expandable valve framework 8, it is possible to use non-woven cellulose that has been hot-pressed in parts. This involves designing the nonwoven fabric so that it has an inside skirt area 9 and an outside 10 skirt area, such as have already been shown as exam-
25 ples in Figures 2 and 3. This inside skirt area 9 is hot-pressed and accordingly non-swella-ble. This skirt area is firmly sutured from inside with the balloon-expandable stent frame 3. The outside skirt area 10 is turned around the inflow area I and sutured to frame 3 from outside. This outside skirt area 10 is made so that the cellulose in the area of the suture points 11 is non-swella-ble.

30

Patent Claims

1. A process for producing a storable and swellable molded body (1) out of bacterial cellulose, this process comprising the following steps:
 - 5 i) Providing a molded body (1) made of bacterial cellulose;
 - ii) Mechanical pressing of parts of the molded body (1) at temperatures in the range of 10°C to 100°C and pressing in the range of 0.0005 to 1.5 MPa for 10-200 min.;
 - iii) Treating the pressed molded body (1) with a solution consisting of:
10 20 weight % to 50 weight % glycerol and 50 weight % to 80 weight % of a C1-C3 alcohol/water mixture; and
 - iv) Drying the treated molded body (1).
2. The process according to claim 1, wherein the temperature in step ii) lies in the range
15 from 80°C to 100°C and the pressure preferably lies in the range from 1.5 kPa and 2 kPa.
3. A storable molded body (1) made of bacterial cellulose, produced by a process according to one of the preceding claims.
20
4. A heart valve implant comprising a supporting stent (3), a heart valve element, and a skirt, wherein the skirt comprises at least one molded body (1) according to claim 3 or being formed of at least one molded body (1).
- 25 5. The heart valve implant according to claim 4, wherein the at least one molded body (1) has at least one area (11) that has lower swelling capacity than an adjacent area (2) of the molded body (1).
6. The heart valve implant according to claim 4 or 5, wherein the skirt comprises an
30 area for sealing paravalvular leakages.

7. The heart valve implant according to one of claims 4 to 6, wherein the skirt is attached in the luminal and/or abluminal area of the supporting stent (3).
8. The heart valve implant according to one of claims 4 to 7, wherein the skirt runs in
5 the luminal (9) and abluminal area (10) of the supporting stent (3), the skirt having reduced swelling capacity in the luminal area (9) and higher swelling capacity in at least parts of the abluminal area (10).
9. The heart valve implant according to one of claims 4 to 7, wherein the skirt is at-
10 tached in the luminal area and comprises multiple molded bodies, the molded bodies being attached between the stent framework and the skirt running in the luminal area.
10. The heart valve implant according to claim 9, wherein the multiple molded bodies
15 are arranged in such a way that molded parts attached next to one another border one another so as to form at least one closed ring in the peripheral direction of the skirt.
11. The heart valve implant according to one of claims 9 or 10, wherein the borders of
the molded body (1) run at least partly on the stent struts (3a, 3b, 3c, 3d) of the sup-
20 porting stent (3).
12. The heart valve implant according to one of claims 4 to 7, wherein the skirt is at-
tached in the luminal area of the supporting stent and wherein the areas of the skirt
that run under the stent struts of the supporting stent have reduced swelling capacity.
- 25 13. The heart valve implant according to one of claims 4 to 7, wherein the skirt runs in
the luminal and abluminal area of the supporting stent and is alternately braided
around the stent struts of the supporting stent in the form of at least one band running
around the circumference, and wherein the areas of the skirt that run on the luminal
side under the stent struts of the supporting stent have reduced swelling capacity.

14. The heart valve implant according to one of claims 4 to 13, wherein the heart valve element comprises at least one heart valve leaflet made of an inventive molded body as described in claim 3.
- 5 15. The heart valve implant according to claim 14, wherein the heart valve element comprises three heart valve leaflets made of a molded body as described in claim 3.

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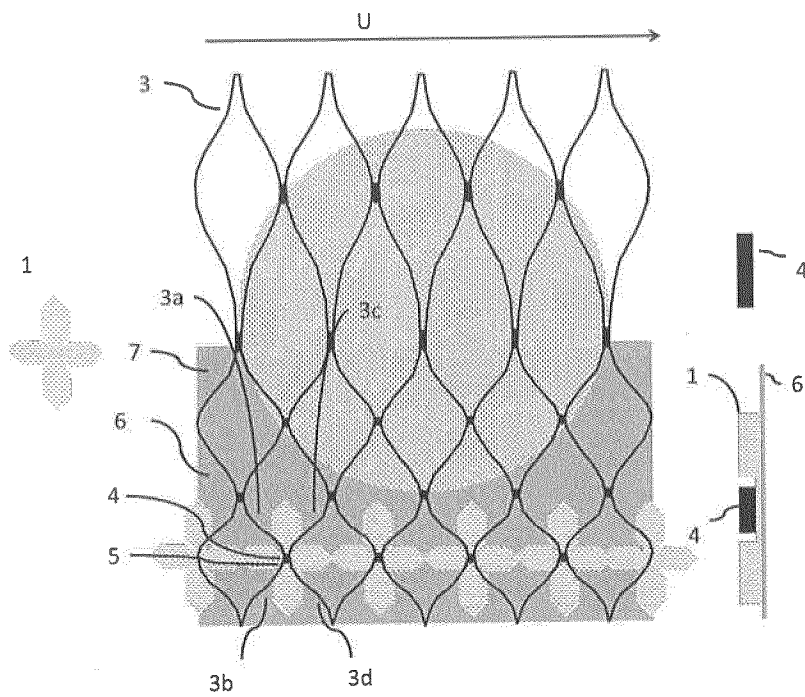


FIG. 1a

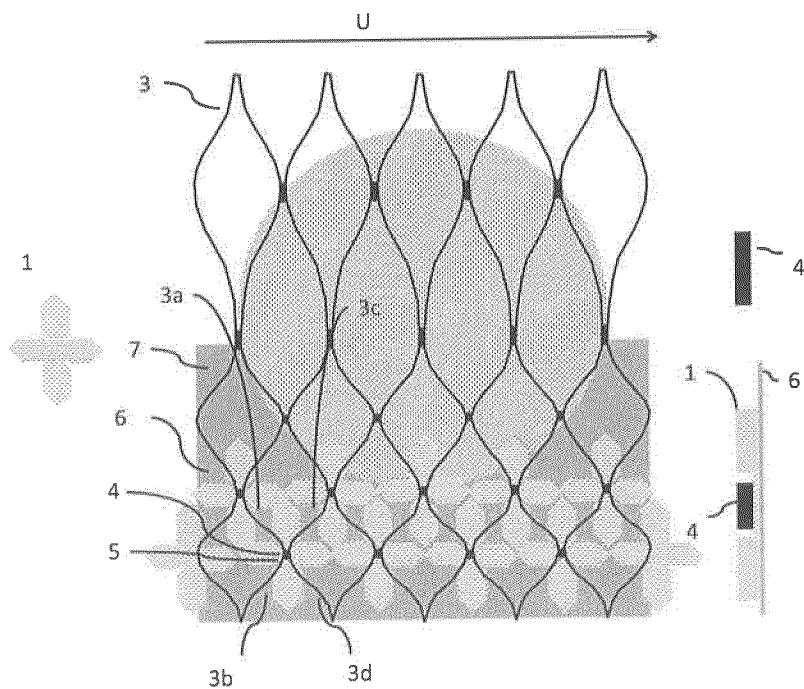


FIG. 1b

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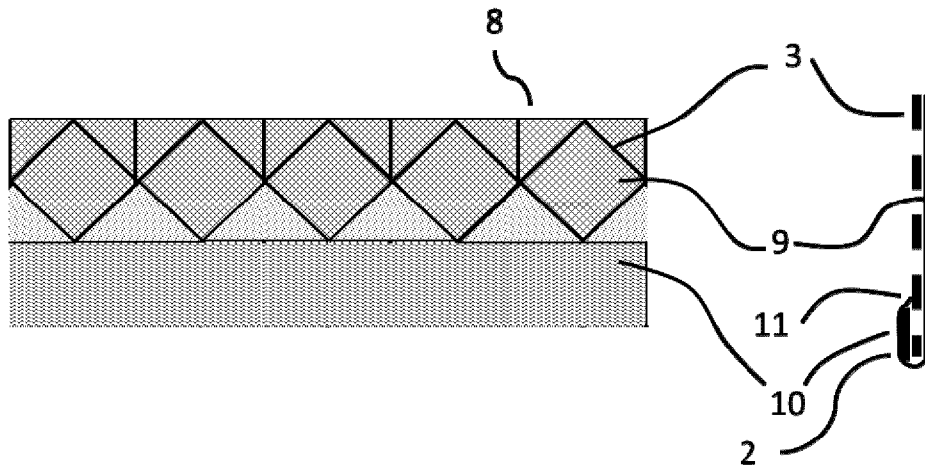


FIG. 2

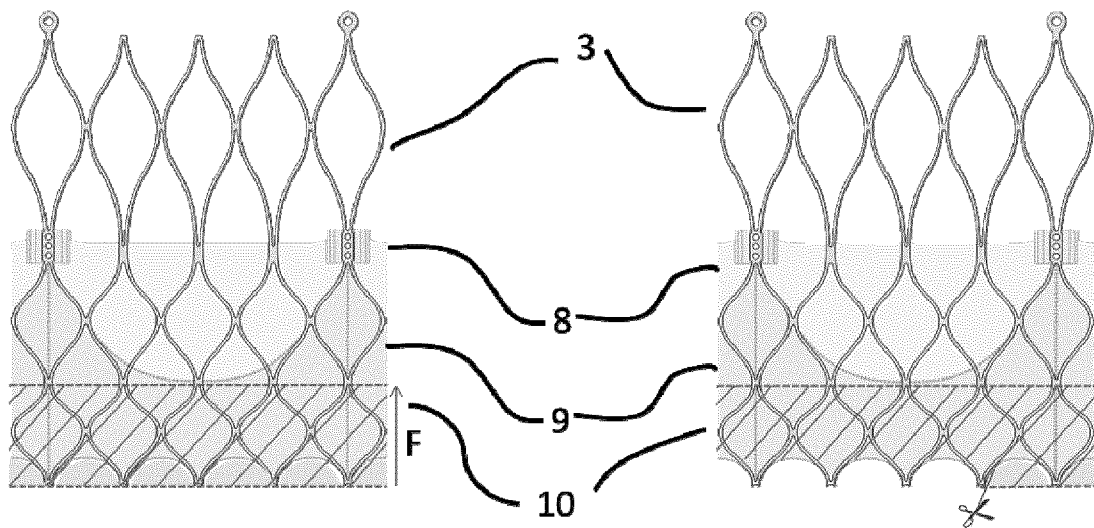
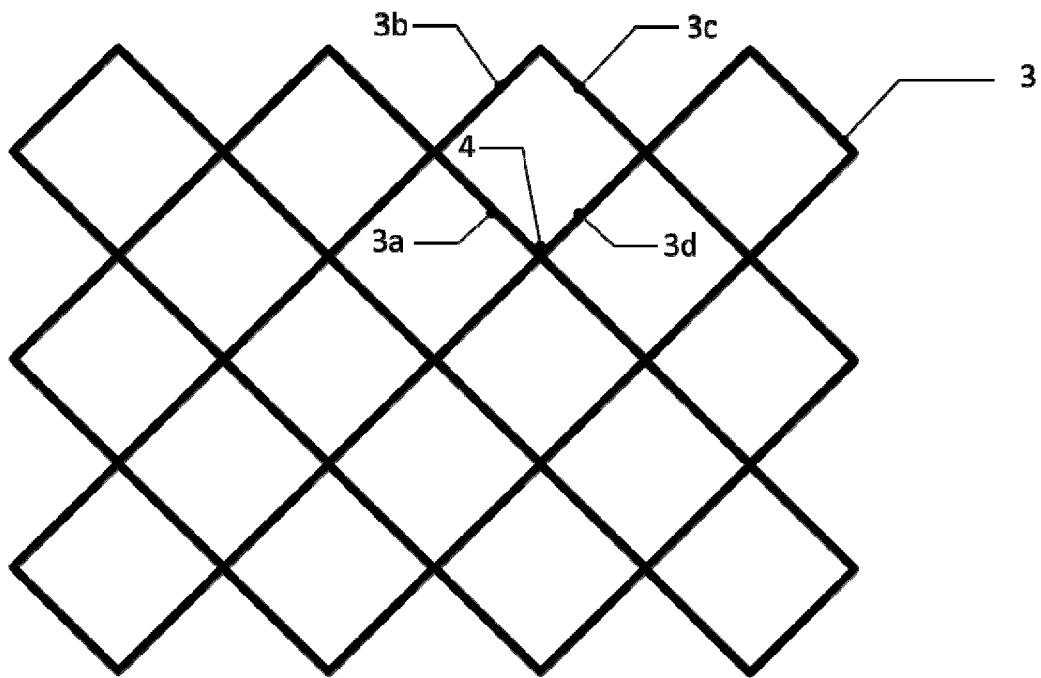
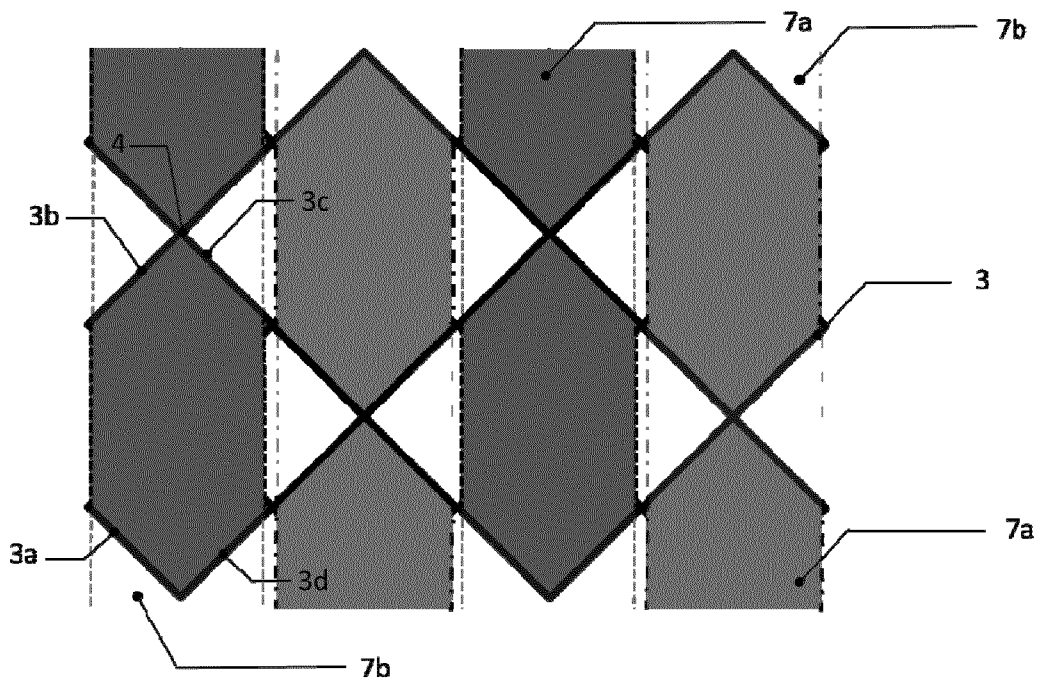


FIG. 3

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**FIG. 4****FIG. 5**

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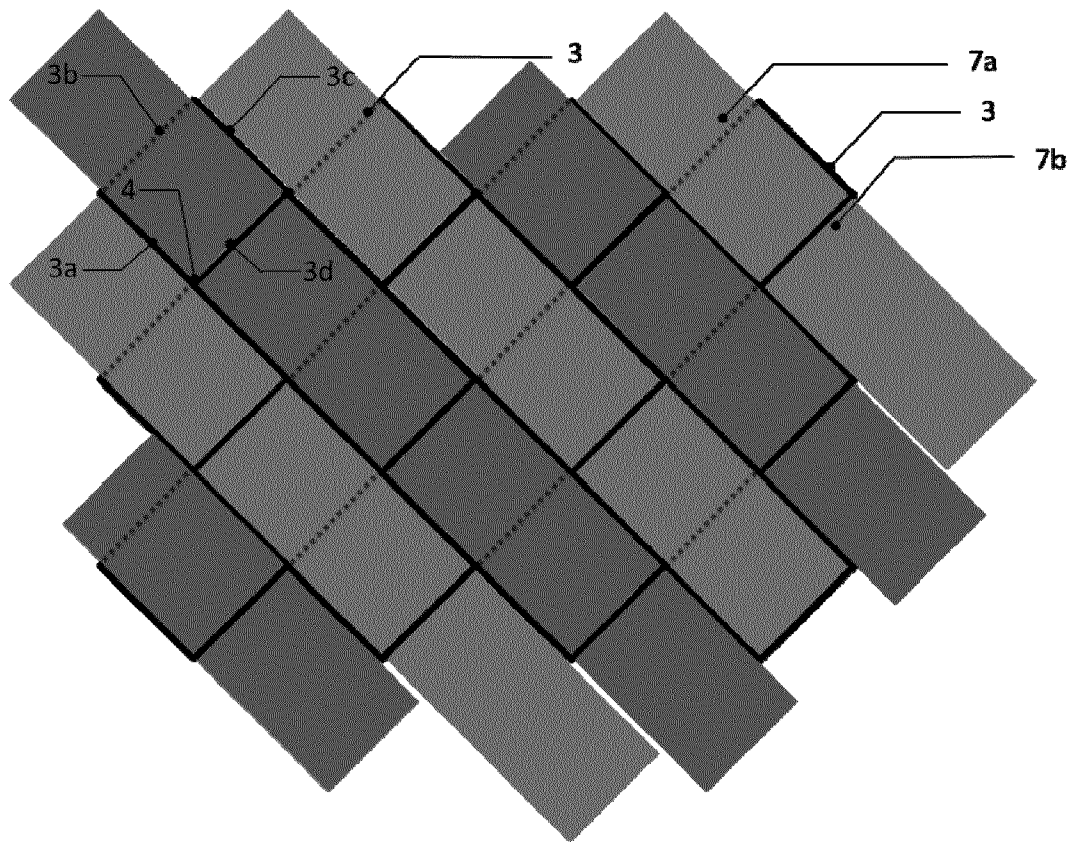


FIG. 6

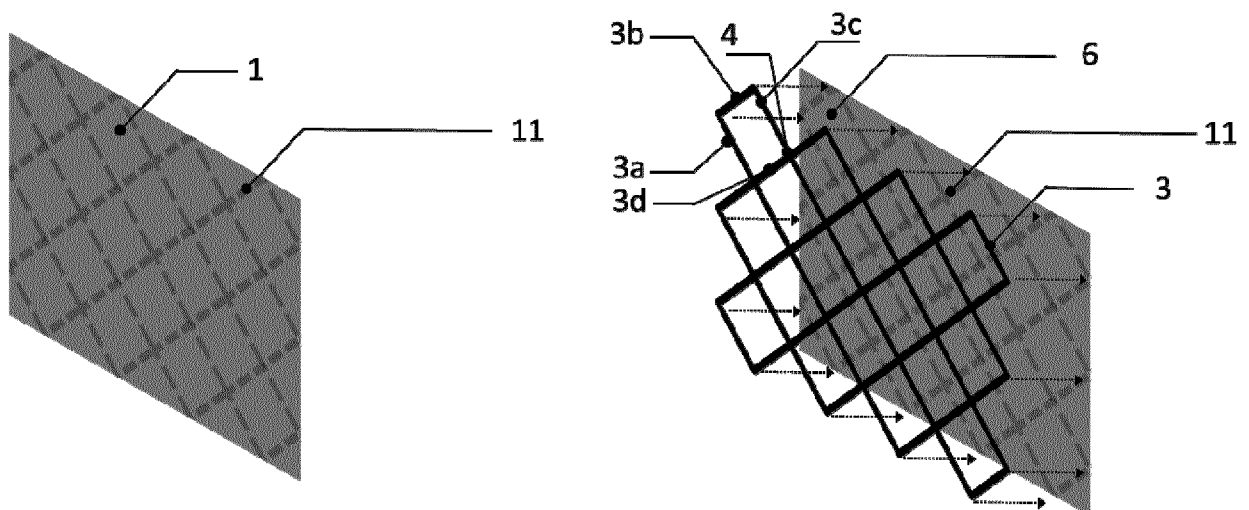


FIG. 7

INTERNATIONAL SEARCH REPORT

International application No
PCT/EP2015/077464A. CLASSIFICATION OF SUBJECT MATTER
INV. A61L31/04
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
A61L

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 4 655 758 A (RING DAVID F [US] ET AL) 7 April 1987 (1987-04-07) column 2, line 11 - line 15 column 2, line 32 - column 3, line 6 column 5, lines 28-41, 58-64 column 6, line 46 - line 60 column 7, line 5 - line 11 example 1 ----- -/--	1-3



Further documents are listed in the continuation of Box C.



See patent family annex.

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Date of the actual completion of the international search

15 February 2016

Date of mailing of the international search report

23/02/2016

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Dudás, Eszter

INTERNATIONAL SEARCH REPORT

International application No

PCT/EP2015/077464

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	<p>Mohammadi H ET AL: "Design and simulation of a poly(vinyl alcohol)-bacterial cellulose nanocomposite mechanical aortic heart valve prosthesis. - PubMed - NCBI", 1 August 2009 (2009-08-01), XP055249955, Retrieved from the Internet: URL:http://www.ncbi.nlm.nih.gov/pubmed/19743636?dopt=Abstract [retrieved on 2016-02-15] abstract</p>	4-15
A	<p>US 2013/331929 A1 (MITRA ASHISH SUDHIR [AU] ET AL) 12 December 2013 (2013-12-12) page 2, paragraph 0021 page 3, paragraph 0022</p>	4-15
A	<p>US 2009/222085 A1 (KUMAR VIJAY [US]) 3 September 2009 (2009-09-03) page 1, paragraphs 0001,0009, 0010</p>	1-15

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/EP2015/077464

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 4655758	A	07-04-1987	AU 5935986 A 08-01-1987
			BR 8602944 A 17-03-1987
			CA 1283099 C 16-04-1991
			DK 305086 A 28-12-1986
			EP 0206830 A2 30-12-1986
			JP 2641428 B2 13-08-1997
			JP 2703531 B2 26-01-1998
			JP S6214787 A 23-01-1987
			JP H08260310 A 08-10-1996
			MX 163664 B 11-06-1992
			NZ 216560 A 29-08-1989
			US 4655758 A 07-04-1987

US 2013331929	A1	12-12-2013	NONE

US 2009222085	A1	03-09-2009	NONE
