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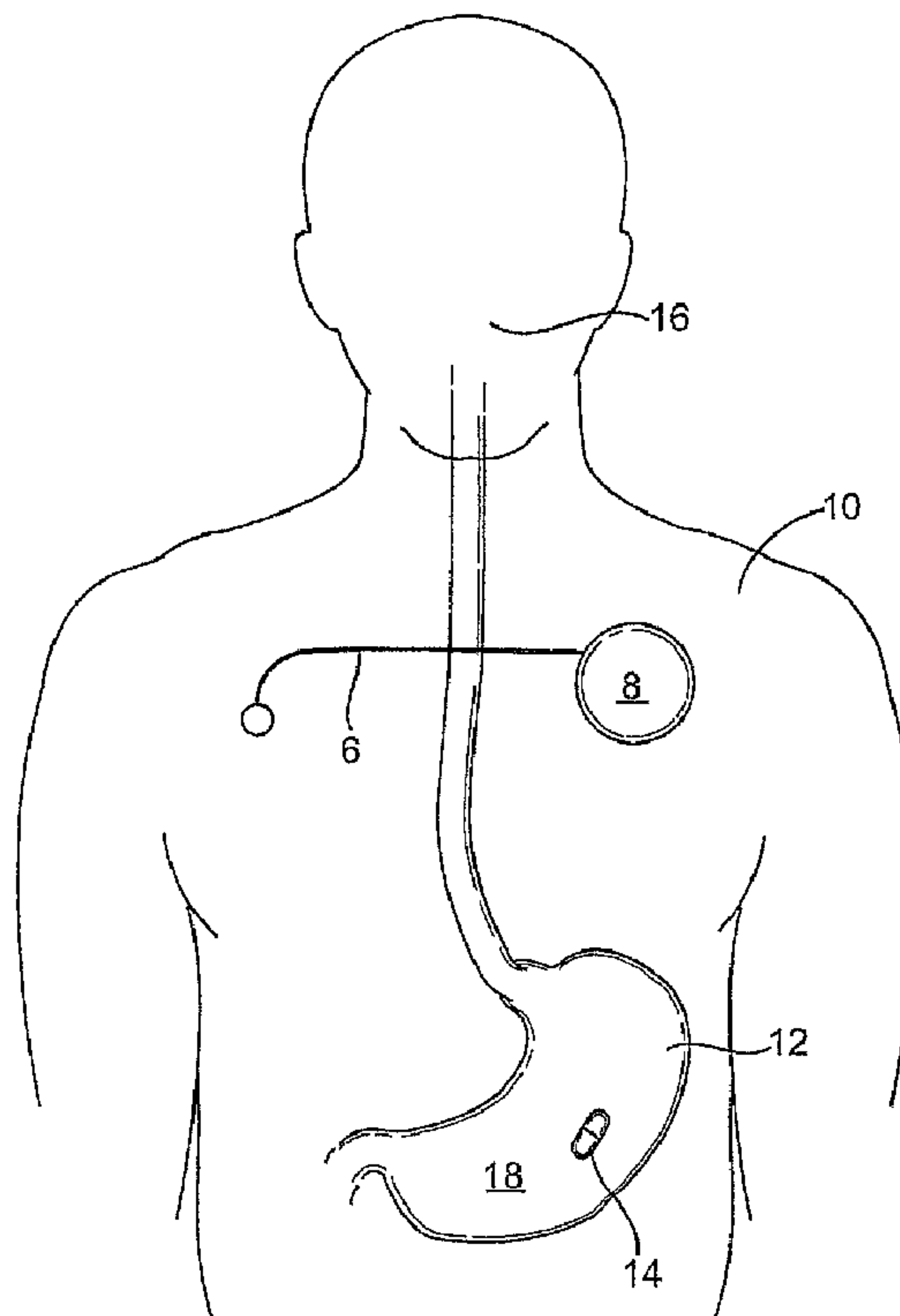
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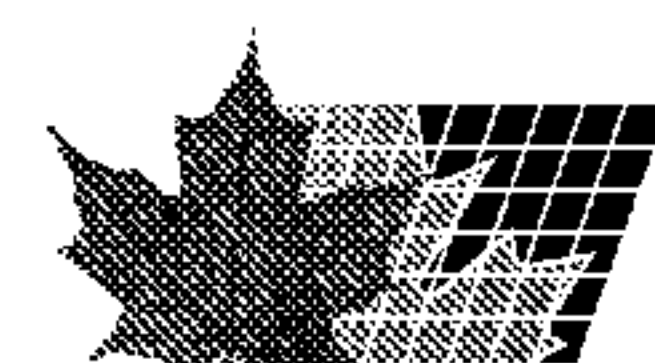
(54) **Titre : SYSTÈME PHARMA-INFORMATIQUE**

(54) **Title: PHARMA-INFORMATICS SYSTEM**



(57) **Abrégé/Abstract:**

Compositions, systems and methods that allow for the detection of the actual physical delivery of a pharmaceutical agent to a body are provided. Embodiments of the compositions include an identifier and an active agent. The invention finds use in a variety of



(57) **Abrégé(suite)/Abstract(continued):**

different applications, including but not limited to, monitoring of therapeutic regimen compliance, tracking the history of pharmaceutical agents, etc.

Abstract

Compositions, systems and methods that allow for the detection of the actual physical delivery of a pharmaceutical agent to a body are provided. Embodiments of the compositions include an identifier and an active agent. The invention finds use in a variety of different applications, including but not limited to, monitoring of therapeutic regimen compliance, tracking the history of pharmaceutical agents, etc.

PHARMA-INFORMATICS SYSTEM

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BACKGROUND

15 The present Invention relates generally to medical apparatus and methods. More specifically, the present invention relates to apparatus and methods for automatic identification of ingestion or other actual, physical administration of a pharmaceutical material.

20 Prescription medications are effective remedies for many patients when taken properly, e.g., according to instructions. However, studies have shown that, on average, about 50% of patients do not comply with prescribed medication regimens. A low rate of compliance with medication regimens results in a large number of hospitalizations and admissions to nursing homes every year. In the United States alone, it has recently been estimated that the cost to the resulting
25 from patient non-compliance is reaching \$100 billion annually.

30 Consequently, various methods and apparatus have been made available to improve patient compliance with prescribed regimens in efforts to improve patient health. To date, many different types of "smart" packaging devices have been developed. In some cases, such devices automatically dispense the appropriate pill. In other cases, there are electronic controls that detect and record when the pill is taken out of the box.

While devices and protocols have been developed for improving patient compliance, there is continued interest in the development of new ways of monitoring patient compliance.

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SUMMARY

The present invention allows, for the first time, the specific identification of pharmaceutical pills and other types of pharmaceutical delivery systems, such as skin diffusion patches, so that the actual, physical delivery of the pharmaceutical into the body can be automatically detected and this information stored.

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Because the inventive automatic reporting of physical drug administration does not require patient or clinician input, it avoids many of the inaccuracies which introduce uncertainty in current drug administration monitoring systems. These inventive features are particularly critical when a patient's compliance or mental capacity are a consideration, such as in the administration of psychotropic drugs.

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The present invention also allows for the identification of sources of illicit drugs for law enforcement purposes.

Embodiments of the invention include compositions having: an active agent; an identifier and a pharmaceutically acceptable carrier. In one embodiment of the present invention, an ingestible pill is made identifiable by providing an electronic microchip as part of the pill structure. In some aspects, the electronic microchip is completely encased within the pill. In this embodiment, the pill broadcasts a signal when it is dissolved in an ionic solution such as stomach fluids. The broadcasted signal is received by another device, e.g., a receiver, either inside or near the body. In turn, the receiver then records that the pill has in fact reached the stomach and is in the process of being dissolved.

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In certain of these embodiments, the signal is an oscillating signal which is picked up by an implanted or topically applied receiver. The implant has one or two electrode(s) that sense the varying signal. The implant is configured so that it can identify the code and record that a specific pill has been ingested at a specific time.

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BRIEF DESCRIPTION OF THE FIGURES

FIG. 1 provides a diagrammatic, exemplary representation of the pill embodiment of the present invention.

FIGS. 2A and **2B** provide a more detailed view of the pill composition shown in **FIG. 1**.

FIGS. 3A to **3C** provide views of different embodiments of signal generation elements of the invention.

5 **FIG. 4** shows diagrammatically the effects of the pill ingestion where some of the pill has eroded away.

FIG. 5 provides a similar arrangement to **FIG. 4**, with a coil rather than two electrodes as the output.

10 **FIGS. 6A** to **6D** provide detail of certain implementations of electronic circuits of various embodiments of the invention.

FIG. 7 provides an oscillator and a counter implementation according to an embodiment of the invention.

FIG. 8 is an additional embodiment of an oscillator where V control modulates the amount of voltage driving the oscillator.

15 **FIG. 9** is an additional embodiment with a simple trickle or asynchronous counter.

FIG. 10 provides a schematic representation of a three terminal, monopole signal generation element according to an embodiment of the invention.

20 **FIGS. 11A** to **13B** are diagrams showing a method for fabricating an identifier according to an embodiment of the invention.

FIG. 14 shows the multiplexer and the addressing system.

FIG. 15 shows a detail of the 4 bit mux of the system shown in **FIG. 14**.

FIG. 16 shows the 1 bit mux in detail that makes up the 4 bit mux.

25 **FIG. 17** is an additional monopole embodiment of a signal generation element.

FIG. 18A is an exemplary schematic diagram of a signal-transmission driver circuit that transmits a signal at a fixed frequency, in accordance with one embodiment of the present invention.

30 **FIG. 18B1-18B2** provides an exemplary schematic diagram of a receiver circuit, in accordance with one embodiment of the present invention.

FIG. 19 shows one exemplary split (i.e., segmented) battery design, in accordance with one embodiment of the present invention.

FIG. 20 shows one exemplary design of the driver circuit that uses split battery electrodes for transmission, in accordance with one embodiment of the present invention.

FIG. 21 shows one exemplary split battery design with a split cathode, in accordance with one embodiment of the present invention.

FIG. 22 shows one exemplary design where the battery electrodes for the driver circuit are coupled to the driver circuit via two external wires, in accordance with one embodiment of the present invention.

FIG. 23 shows the principle of an experiment with a split battery configuration.

FIG. 24 shows the performance of a pair of split batteries.

DETAILED DESCRIPTION

The present invention provides the clinician an important new tool in their therapeutic armamentarium: automatic detection and identification of pharmaceutical agents actually delivered into the body. The applications of this new information device and system are multi-fold. By example, when used in concert with other medical sensing devices, correlation between drug delivery, batch and dosage can be correlated to a physiological response. In this manner, optimal pharma-therapeutic regimens may be formulated by the clinician. By example, cardiac stimulating drugs can be titrated to the most appropriate dosages, minimizing side effects such as cardiac muscle exhaustion and rebound effects among others, and optimizing both dosage and timing for each, individual patient.

Assessment of a range of alternate medications is made possible by the present invention without resort to awaiting overt clinical sequel of treatment, many of which can be seriously adverse. By example, positive effects would be quickly ascertainable without being obscured by more random factors. Negative responses, such as changes in blood pressure, would become clearly evident as drug related or independent above background physiologic variation.

The ability to document the ingestion of a drug or other actual exposure of the body to a medication has many important clinical applications. In the simplest form, this technique provides accurate data of when a pill has been taken and

which pill has been taken. This allows the precise determination of which pill was taken at a specific point in time. Such monitoring capability assures patients are taking the prescribed medication correctly. This information avoids the potential for over prescription of medications that are not actually being taken. By example, if pain killers are intended to be administered to a patient, it is possible to verify that the patient did in fact take those pain killers in a certain period of time. This is an important tool in limiting the illicit sale of unconsumed drugs to an unintended party. In the case of cardio vascular pills, the clinician or care giver is able to verify that the amount of the drug was taken has been taken at approximately the right point and time. Thus, the true efficacy of the drug can be accurately evaluated. Proper administration and patient compliance is especially critical in Alzheimer's, psychiatric, and alcohol aversion drugs, and in the treatment of rest home residents. In the case of accidental and other overdoses situations, the intervening clinician will be able to discern how far the ingestion has proceeded, and how many pills are involved.

In one clinical arena, the present invention allows, in concert with other sensing device developed by some of the present inventors, the measurement and assessment of the cardiac response to those medications. These co-employed sensing devices can be those enumerated below, among others. Other sensing technology developed by some of the present inventors allows measurement of heart health and cardiac efficiency. Using these tools in concert with the present inventive device, the clinician will be able to compare the response of the heart and body to the administered pharmaceutical.

The data provided by the present invention can optionally be recorded over time. The recording system records synchrony or conduction velocity of a signal going through cardiac tissue and how that is mediated by the presence of a certain medication. This unique data is made possible by the present invention since it can determine electronically exactly when the pill or other medication was being absorbed into the body.

From this innovative data, the present invention provides the clinician an accurate dose response curve showing the response to that medication and the timing of the digestion of the pill. Such innovative data has many applications. For instance, the clinician now has the ability to determine which patients have no response to the medicine in the pill. In a study situation, such patients can be

removed from a study or a test of the clinical utility of a certain medication. This provides that only people who have a beneficial response to a certain medication are retained in the trial. This feature will improve the efficacy of medications and to reduce the amount of medications that people take that are not being useful. It
5 may also be used in trials to determine which patients actually consumed the medicine, and which did not.

In more standard clinical environments, this unique data allows careful selection and titration of drug administration without resort to more overt physical symptoms to ascertain contraindications, efficacy, and optimal dosage levels.

10 The present invention provides a record for emergency room technicians or doctors when a patient is admitted to a hospital so that the patient's status can be accurately ascertained. Dosage events within the last hour or day prior to admission, and the identity of the last medication, will be immediately available.

The clinician obtains this information through simple interrogation of the
15 implanted or portable device. This device would tell them without any uncertainty what pills have been taken. As the inventive technology becomes more wide spread, this data will become more regularly available. The present inventive microchips described below are sufficiently inexpensive when put into standard production that most or all pharmaceuticals will be fitted with them as a matter of
20 course.

In other embodiments of the inventive microchips, the chips can be fitted with coils, susceptible of interrogation without being dissolved in the body. This is accomplished by transmitting RF energy into the coil in such a way that the inquirer will be apprised of the presence and identity of a pill before it is ingested.

25 In an additional embodiment of the present invention, a "smart box" is provided that can interrogate each pill and ascertain its address. The box can write a distinctive product number or product code so that every single pill ever made is provided with a unique identifier. Fuses, for example, may be selectively destroyed so the addresses may be detected electrically or optically. Particularly
30 in the case of controlled substances, such as a narcotic, this will be important in limiting the illegal use of previously legitimate medicines. The present invention makes it possible to identify precisely who bought such a pill from the authorized pharmacist. This use of the present invention will rein in the number of illicit uses of controlled substances on the market place.

In further describing the invention in greater detail, embodiments of the compositions are reviewed first, followed by a discussion of systems including the subject compositions, methods of using the subject compositions and systems and various illustrative applications in which the compositions and methods find use. Also reviewed in greater detail below are kits that include the subject compositions.

COMPOSITIONS

Embodiments of the invention include active agent compositions having an identifier stably associated therewith. In certain embodiments, the compositions are disrupted upon administration to a subject. As such, in certain embodiments, the compositions are physically broken, e.g., dissolved, degraded, eroded, etc., following delivery to a body, e.g., via ingestion, injection, etc. The compositions of these embodiments are distinguished from devices that are configured to be ingested and survive transit through the gastrointestinal tract substantially, if not completely, intact. While the compositions of these embodiments are themselves disrupted upon administration, components of the composition, e.g., the identifier, may survive transit of the gastrointestinal tract, e.g., as described in greater detail below.

In certain embodiments, the compositions include an active agent/carrier component and an identifier. Each of these different components are reviewed separately in greater detail below.

Active Agent/Carrier Component

The subject compositions include an active agent/carrier component. By "active agent/carrier component" is meant a composition, which may be a solid or fluid (e.g., liquid), which has an amount of active agent, e.g., a dosage, present in a pharmaceutically acceptable carrier. The active agent/carrier component may be referred to as a "dosage formulation."

Active Agent

"Active agent" includes any compound or mixture of compounds which produces a physiological result, e.g., a beneficial or useful result, upon contact

with a living organism, e.g., a mammal, such as a human. Active agents are distinguishable from such components as vehicles, carriers, diluents, lubricants, binders and other formulating aids, and encapsulating or otherwise protective components. The active agent may be any molecule, as well as binding portion or
5 fragment thereof, that is capable of modulating a biological process in a living subject. In certain embodiments, the active agent may be a substance used in the diagnosis, treatment, or prevention of a disease or as a component of a medication. In certain embodiments, the active agent may be a chemical substance, such as a narcotic or hallucinogen, which affects the central nervous
10 system and causes changes in behavior.

The active agent (i.e., drug) is capable of interacting with a target in a living subject. The target may be a number of different types of naturally occurring structures, where targets of interest include both intracellular and extracellular targets. Such targets may be proteins, phospholipids, nucleic acids
15 and the like, where proteins are of particular interest. Specific proteinaceous targets of interest include, without limitation, enzymes, e.g. kinases, phosphatases, reductases, cyclooxygenases, proteases and the like, targets comprising domains involved in protein-protein interactions, such as the SH2, SH3, PTB and PDZ domains, structural proteins, e.g. actin, tubulin, etc.,
20 membrane receptors, immunoglobulins, e.g. IgE, cell adhesion receptors, such as integrins, etc, ion channels, transmembrane pumps, transcription factors, signaling proteins, and the like.

The active agent (i.e., drug) may include one or more functional groups necessary for structural interaction with the target, e.g., groups necessary for
25 hydrophobic, hydrophilic, electrostatic or even covalent interactions, depending on the particular drug and its intended target. Where the target is a protein, the drug moiety may include functional groups necessary for structural interaction with proteins, such as hydrogen bonding, hydrophobic-hydrophobic interactions, electrostatic interactions, etc., and may include at least an amine, amide,
30 sulfhydryl, carbonyl, hydroxyl or carboxyl group, such as at least two of the functional chemical groups.

Drugs of interest may include cyclical carbon or heterocyclic structures and/or aromatic or polyaromatic structures substituted with one or more of the above functional groups. Also of interest as drug moieties are structures found

among biomolecules, including peptides, saccharides, fatty acids, steroids, purines, pyrimidines, derivatives, structural analogs or combinations thereof. Such compounds may be screened to identify those of interest, where a variety of different screening protocols are known in the art.

5 The drugs may be derived from a naturally occurring or synthetic compound that may be obtained from a wide variety of sources, including libraries of synthetic or natural compounds. For example, numerous means are available for random and directed synthesis of a wide variety of organic compounds and biomolecules, including the preparation of randomized
10 oligonucleotides and oligopeptides. Alternatively, libraries of natural compounds in the form of bacterial, fungal, plant and animal extracts are available or readily produced. Additionally, natural or synthetically produced libraries and compounds are readily modified through conventional chemical, physical and biochemical means, and may be used to produce combinatorial libraries. Known
15 pharmacological agents may be subjected to directed or random chemical modifications, such as acylation, alkylation, esterification, amidification, etc. to produce structural analogs.

As such, the drug may be obtained from a library of naturally occurring or synthetic molecules, including a library of compounds produced through
20 combinatorial means, i.e., a compound diversity combinatorial library. When obtained from such libraries, the drug moiety employed will have demonstrated some desirable activity in an appropriate screening assay for the activity. Combinatorial libraries, as well as methods for producing and screening such libraries, are known in the art and described in US Patent Nos: 5,741,713;
25 5,734,018; 5,731,423; 5,721,099; 5,708,153; 5,698,673; 5,688,997; 5,688,696; 5,684,711; 5,641,862; 5,639,603; 5,593,853; 5,574,656; 5,571,698; 5,565,324; 5,549,974; 5,545,568; 5,541,061 ; 5,525,735; 5,463,564; 5,440,016; 5,438,119; 5,223,409.

Broad categories of active agents of interest include, but are not limited to:
30 cardiovascular agents; pain-relief agents, e.g., analgesics, anesthetics, anti-inflammatory agents, etc.; nerve-acting agents; chemotherapeutic (e.g., anti-neoplastic) agents; etc.

In certain embodiments, the active agent is a cardiovascular agent, i.e., an agent employed in the treatment of cardiovascular or heart conditions. In certain

embodiments, the active agent is a cardiovascular agent, i.e., an agent employed in the treatment of cardiovascular or heart conditions. Cardiovascular agents of interest include, but are not limited to: cardioprotective agents, e.g., Zinecard (dexrazoxane); blood modifiers, including anticoagulants (e.g., coumadin (warfarin sodium), fragmin (dalteparin sodium), heparin, innohep (tinzaparin sodium), lovenox (enoxaparin sodium), orgaran (danaparoid sodium)) antiplatelet agents (e.g., aggrasta (tirofiban hydrochloride), aggrenox (aspirin/extended release dipyridamole), agrylin (anagrelide hydrochloride), ecotrin (acetylsalicylic acid), folan (epoprostenol sodium), halfprin (enteric coated aspirin), integrilin (eptifibatide), persantine (dipyridamole USP), plavix (clopidogrel bisulfate), pletal (cilostazol), reopro (abciximab), ticlid (ticlopidine hydrochloride)), thrombolytic agents (activase (alteplase), retavase (reteplase), streptase (streptokinase)); adrenergic blockers, such as cardura (doxazosin mesylate), dibenzyline (phenoxybenzamine hydrochloride), hytrin (terazosin hydrochloride), minipress (prazosin hydrochloride), minizide (prazosin hydrochloride/polythiazide); adrenergic stimulants, such as aldoclor (methyldopa – chlorothiazide), aldomet (methyldopa, methyldopate HCl), aldoril (methyldopa – hydrochlorothiazide), catapres (clonidine hydrochloride USP, clonidine), clorpres (clonidine hydrochloride and chlorthalidone), combipres (clonidine hydrochloride/ chlorthalidone), tenex (guanfacine hydrochloride); alpha/bet adrenergic blockers, such as coreg (carvedilol), normodyne (labetalol hydrochloride); angiotensin converting enzyme (ACE) inhibitors, such as accupril (quinapril hydrochloride), aceon (perindopril erbumine), altace (ramipril), captopril, lotensin (benazepril hydrochloride), mavik (trandolapril), monopril (fosinopril sodium tablets), prinivil (lisinopril), univasc (moexipril hydrochloride), vasotec (enalaprilat, enalapril maleate), zestril (lisinopril); angiotensin converting enzyme (ACE) inhibitors with calcium channel blockers, such as lexxel (enalapril maleate – felodipine ER), lotrel (amlodipine and benazepril hydrochloride), tarka (trandolapril/verapamil hydrochloride ER); angiotensin converting enzyme (ACE) inhibitors with diuretics, such as accuretic (quinapril HCl/hydrochlorothiazide), lotensin (benazepril hydrochloride and hydrochlorothiazide USP), prinizide (lisinopril–hydrochlorothiazide), uniretic (moexipril hydrochloride/hydrochlorothiazide), vaseretic (enalapril maleate – hydrochlorothiazide), zestoretic (lisinopril and hydrochlorothiazide); angiotensin II receptor antagonists, such as atacand

(candesartan cilexetil), avapro (irbesartan), cozaar (losartan potassium), diovan (valsartan), micardis (telmisartan), teveten (eprosartan mesylate); angiotensin II receptor antagonists with diuretics, such as avalide (irbesartan – hydrochlorothiazide), diovan (valsartan and hydrochlorothiazide), hyzaar (losartan potassium – hydrochlorothiazide); antiarrhythmics, such as Group I (e.g., mexitil (mexiletine hydrochloride, USP), norpace (disopyramide phosphate), procanbid (procainamide hydrochloride), quinaglute (quinidine gluconate), quinidex (quinidine sulfate), quinidine (quinidine gluconate injection, USP), rythmol (propafenone hydrochloride), tambocor (flecainide acetate), tonocard (tocainide HCl)), Group II (e.g., betapace (sotalol HCl), brevibloc (esmolol hydrochloride), inderal (propranolol hydrochloride), sectral (acebutolol hydrochloride)), Group III (e.g., betapace (sotalol HCl), cordarone (amiodarone hydrochloride), corvert (ibutilide fumarate injection), pacerone (amiodarone HCl), tikosyn (dofetilide)), Group IV (e.g., calan (verapamil hydrochloride), cardizem (diltiazem HCl), as well as adenocard (adenosine), lanoxicaps (digoxin), lanoxin (digoxin)); antilipemic acids, including bile acid sequestrants (e.g., colestid (micronized colestipol hydrochloride), welchol (colesevelam hydrochloride)), fibric acid derivatives (e.g., atromid (clofibrate), lopid (gemfibrozil tablets, USP), tricor (fenofibrate capsules)), HMG-CoA reductase inhibitors (e.g., baycol (cerivastatin sodium tablets), lescol (fluvastatin sodium), lipitor (atorvastatin calcium), mevacor (lovastatin), pravachol (pravastatin sodium), zocor (simvastatin)), Nicotinic Acid (e.g., Niaspan (niacin extended release tablets)); beta adrenergic blocking agents, e.g., betapace (sotalol HCl), blocadren (timolol maleate), brevibloc (esmolol hydrochloride), cartrol (carteolol hydrochloride), inderal (propranolol hydrochloride), kerlone (betaxolol hydrochloride), nadolol, sectral (acebutolol hydrochloride), tenormin (atenolol), toprol (metoprolol succinate), zebeta (bisoprolol fumarate); beta adrenergic blocking agents with diuretics, e.g., corzide (nadolol and bendroflumethiazide tablets), inderide (propranolol hydrochloride and hydrochlorothiazide), tenoretic (atenolol and chlorthalidone), timolide (timolol maleate – hydrochlorothiazide), ziac (bisoprolol fumarate and hydrochlorothiazide); calcium channel blockers, e.g., adalat (nifedipine), calan (verapamil hydrochloride), cardene (nicardipine hydrochloride), cardizem (diltiazem HCl), covera (verapamil hydrochloride), isoptin (verapamil hydrochloride), nimotop (nimodipine), norvasc (amlodipine besylate), plendil (felodipine), procardia

(nifedipine), sular (nisoldipine), tiazac (diltiazem hydrochloride), vascor (bepridil hydrochloride), verelan (verapamil hydrochloride); diuretics, including carbonic anhydrase inhibitors (e.g., daranide (dichlorphenamide)), combination diuretics (e.g., aldactazide (spironolactone with hydrochlorothiazide), dyazide (triamterene and hydrochlorothiazide), maxzide (triamterene and hydrochlorothiazide), moduretic (amiloride HCl - hydrochlorothiazide)), loop diuretics (demadex (torsemide), edecrin (ethacrynic acid, ethacrynate sodium), furosemide), potassium-sparing diuretics (aldactone (spironolactone), dyrenium (triamterene), midamor (amiloride HCl)), thiazides & related diuretics (e.g., diucardin (hydroflumethiazide), diuril (chlorothiazide, chlorothiazide sodium), enduron (methyclothiazide), hydrodiuril hydrochlorothiazide), indapamide, microzide (hydrochlorothiazide) mykrox (metolazone tablets), renese (polythi-azide), thalitone (chlorthalidone, USP), zaroxolyn (metolazone)); inotropic agents, e.g., digitek (digoxin), dobutrex (dobutamine), lanoxicaps (digoxin), lanoxin (digoxin), primacor (milrinone lactate); activase (alteplase recombinant); adrenaline chloride (epinephrine injection, USP); demser (metyrosine), inversine (mecamylamine HCl), reopro (abciximab), retavase (reteplase), streptase (streptokinase), tnkase (tenecteplase); vasodilators, including coronary vasodilators (e.g., imdur (isosorbide mononitrate), ismo (isosorbide mononitrate), isordil (isosorbide dinitrate), nitrodur (nitroglycerin), nitrolingual (nitroglycerin lingual spray), nitrostat (nitroglycerin tablets, USP), sorbitrate (isosorbide dinitrate)), peripheral vasodilators & combinations (e.g., corlopam (fenoldopam mesylate), fiolan (epoprostenol sodium), primacor (milrinone lactate)), vasopressors, e.g., aramine (metaraminol bitartrate), epipen (EpiPen 0.3 mg brand of epinephrine auto injector, EpiPen Jr. 0.15 mg brand of epinephrine auto injector), proamatine (midodrine hydrochloride); etc.

In certain embodiments, specific drugs of interest include, but are not limited to: psychopharmacological agents, such as (1) central nervous system depressants, e.g. general anesthetics (barbiturates, benzodiazepines, steroids, cyclohexanone derivatives, and miscellaneous agents), sedative-hypnotics (benzodiazepines, barbiturates, piperidinediones and triones, quinazoline derivatives, carbamates, aldehydes and derivatives, amides, acyclic ureides, benzazepines and related drugs, phenothiazines, etc.), central voluntary muscle tone modifying drugs (anticonvulsants, such as hydantoins, barbiturates,

oxazolidinediones, succinimides, acylureides, glutarimides, benzodiazepines, secondary and tertiary alcohols, dibenzazepine derivatives, valproic acid and derivatives, GABA analogs, etc.), analgesics (morphine and derivatives, oripavine derivatives, morphinan derivatives, phenylpiperidines, 2,6-methane-3-benzazocaine derivatives, diphenylpropylamines and isosteres, salicylates, p-aminophenol derivatives, 5-pyrazolone derivatives, arylacetic acid derivatives, fenamates and isosteres, etc.) and antiemetics (anticholinergics, antihistamines, antidopaminergics, etc.), (2) central nervous system stimulants, e.g. analeptics (respiratory stimulants, convulsant stimulants, psychomotor stimulants), narcotic antagonists (morphine derivatives, oripavine derivatives, 2,6-methane-3-benzoxacine derivatives, morphinan derivatives) nootropics, (3) psychopharmacologicals, e.g. anxiolytic sedatives (benzodiazepines, propanediol carbamates) antipsychotics (phenothiazine derivatives, thioxanthine derivatives, other tricyclic compounds, butyrophenone derivatives and isosteres, diphenylbutylamine derivatives, substituted benzamides, arylpiperazine derivatives, indole derivatives, etc.), antidepressants (tricyclic compounds, MAO inhibitors, etc.), (4) respiratory tract drugs, e.g. central antitussives (opium alkaloids and their derivatives);

pharmacodynamic agents, such as (1) peripheral nervous system drugs, e.g. local anesthetics (ester derivatives, amide derivatives), (2) drugs acting at synaptic or neuroeffector junctional sites, e.g. cholinergic agents, cholinergic blocking agents, neuromuscular blocking agents, adrenergic agents, antiadrenergic agents, (3) smooth muscle active drugs, e.g. spasmolytics (anticholinergics, musculotropic spasmolytics), vasodilators, smooth muscle stimulants, (4) histamines and antihistamines, e.g. histamine and derivative thereof (betazole), antihistamines (H1-antagonists, H2-antagonists), histamine metabolism drugs, (5) cardiovascular drugs, e.g. cardiotonics (plant extracts, butenolides, pentadienolids, alkaloids from erythrophleum species, ionophores, -adrenoceptor stimulants, etc), antiarrhythmic drugs, antihypertensive agents, antilipidemic agents (clofibric acid derivatives, nicotinic acid derivatives, hormones and analogs, antibiotics, salicylic acid and derivatives), antivaricose drugs, hemostyptics, (6) blood and hemopoietic system drugs, e.g. antianemia drugs, blood coagulation drugs (hemostatics, anticoagulants, antithrombotics, thrombolytics, blood proteins and their fractions), (7) gastrointestinal tract drugs,

e.g. digestants (stomachics, cholaretics), antiulcer drugs, antidiarrheal agents, (8) locally acting drugs;

chemotherapeutic agents, such as (1) anti-infective agents, e.g. ectoparasitocides (chlorinated hydrocarbons, pyrethins, sulfurated compounds),
 5 anthelmintics, antiprotozoal agents, antimalarial agents, antiamebic agents, antileishmanial drugs, antitrichomonal agents, antitrypanosomal agents, sulfonamides, antimycobacterial drugs, antiviral chemotherapeutics, etc., and (2) cytostatics, i.e. antineoplastic agents or cytotoxic drugs, such as alkylating agents, e.g. Mechlorethamine hydrochloride (Nitrogen Mustard, Mustargen, HN2), Cyclophosphamide (Cytovan, Endoxana), Ifosfamide (IFEX), Chlorambucil (Leukeran), Melphalan (Phenylalanine Mustard, L-sarcolysin, Alkeran, L-PAM), Busulfan (Myleran), Thiotepa (Triethylenethiophosphoramide), Carmustine (BiCNU, BCNU), Lomustine (CeeNU, CCNU), Streptozocin (Zanosar) and the like; plant alkaloids, e.g. Vincristine (Oncovin), Vinblastine (Velban, Velbe),
 15 Paclitaxel (Taxol), and the like; antimetabolites, e.g. Methotrexate (MTX), Mercaptopurine (Purinethol, 6-MP), Thioguanine (6-TG), Fluorouracil (5-FU), Cytarabine (Cytosar-U, Ara-C), Azacitidine (Mylosar, 5-AZA) and the like; antibiotics, e.g. Dactinomycin (Actinomycin D, Cosmegen), Doxorubicin (Adriamycin), Daunorubicin (daunomycin, Cerubidine), Idarubicin (Idamycin),
 20 Bleomycin (Blenoxane), Picamycin (Mithramycin, Mithracin), Mitomycin (Mutamycin) and the like, and other anticellular proliferative agents, e.g. Hydroxyurea (Hydrea), Procarbazine (Mutalane), Dacarbazine (DTIC-Dome), Cisplatin (Platinol) Carboplatin (Paraplatin), Asparaginase (Elspar) Etoposide (VePesid, VP-16-213), Amsacrine (AMSA, m-AMSA), Mitotane (Lysodren),
 25 Mitoxantrone (Novatrone), and the like;

antibiotics, such as: aminoglycosides, e.g. amikacin, apramycin, arbekacin, bambarmycins, butirosin, dibekacin, dihydrostreptomycin, fortimicin, gentamicin, isepamicin, kanamycin, micromycin, neomycin, netilmicin, paromycin, ribostamycin, sisomicin, spectinomycin, streptomycin, tobramycin, trospectomycin; amphenicols, e.g. azidamfenicol, chloramphenicol, florfenicol, and theimaphenicol; ansamycins, e.g. rifamide, rifampin, rifamycin, rifapentine, rifaximin; b-lactams, e.g. carbacephems, carbapenems, cephalosporins, cephamycins, monobactams, oxaphems, penicillins; lincosamides, e.g. clindamycin, lincomycin; macrolides, e.g. clarithromycin, dirithromycin,

erythromycin, etc.; polypeptides, e.g. amphotericin, bacitracin, capreomycin, etc.; tetracyclines, e.g. apicycline, chlortetracycline, clomocycline, etc.; synthetic antibacterial agents, such as 2,4-diaminopyrimidines, nitrofurans, quinolones and analogs thereof, sulfonamides, sulfones;

5 antifungal agents, such as: polyenes, e.g. amphotericin B, candicidin, dermostatin, filipin, fungichromin, hachimycin, hamycin, lucensomycin, mepartricin, natamycin, nystatin, pecilocin, perimycin; synthetic antifungals, such as allylamines, e.g. butenafine, naftifine, terbinafine; imidazoles, e.g. bifonazole, butoconazole, chlordanol, chlormidazole, etc., thiocarbamates, e.g. tolciolate, 10 triazoles, e.g. fluconazole, itraconazole, terconazole;

anthelmintics, such as: arecoline, aspidin, aspidinol, dichlorophene, embelin, kosin, naphthalene, niclosamide, pelletierine, quinacrine, alantolactone, amocarzine, amoscanate, ascaridole, bethovenium, bitoscanate, carbon tetrachloride, carvacrol, cyclobendazole, diethylcarbamazine, etc.;

15 antimalarials, such as: acedapsone, amodiaquin, arteether, artemether, artemisinin, artesunate, atovaquone, bebeerine, berberine, chirata, chlorguanide, chloroquine, chlorproguanil, cinchona, cinchonidine, cinchonine, cycloguanil, gentiopicrin, halofantrine, hydroxychloroquine, mefloquine hydrochloride, 3-methylarsacetin, pamaquine, plasmocid, primaquine, pyrimethamine, quinacrine, 20 quinidine, quinine, quinocide, quinoline, dibasic sodium arsenate;

antiprotozoan agents, such as: acranil, tinidazole, ipronidazole, ethylstibamine, pentamidine, acetarsone, aminitroazole, anisomycin, nifuratel, tinidazole, benzidazole, suramin, and the like.

Name brand drugs of interest include, but are not limited to: Rezulin[®], 25 Lovastatin[™], Enalapril[™], Prozac[™], Prilosec[™], Lipotor[™], Claritin[™], Zocor[™], Ciprofloxacin[™], Viagra[™], Crixivan[™], Ritalin[™], and the like.

Drug compounds of interest are also listed in: Goodman & Gilman's, The Pharmacological Basis of Therapeutics (9th Ed) (Goodman et al. eds) (McGraw-Hill) (1996); and 2001 Physician's Desk Reference.

30 Specific compounds of interest also include, but are not limited to:

antineoplastic agents, as disclosed in U.S. Patent no.'s 5880161, 5877206, 5786344, 5760041, 5753668, 5698529, 5684004, 5665715, 5654484, 5624924, 5618813, 5610292, 5597831, 5530026, 5525633, 5525606, 5512678,

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 5 4785085, 476925, 4684747, 4618685, 4611066, 4550187, 4550186, 4544501,
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 4246411, 4214089, 4150231, 4147798, 4056673, 4029661, 4012448;

psycopharmacological/psychotropic agents, as disclosed in U.S. Patent
 no.'s 5192799, 5036070, 4778800, 4753951, 4590180, 4690930, 4645773,
 10 4427694, 4424202, 4440781, 5686482, 5478828, 5461062, 5387593, 5387586,
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 15 4231930, 4194009, 4188388, 4148796, 4128717, 4062858, 4031226, 4020072,
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cardiovascular agents, as disclosed in U.S. Patent no.'s 4966967,
 5661129, 5552411, 5332737, 5389675, 5198449, 5079247, 4966967, 4874760,
 20 4954526, 5051423, 4888335, 4853391, 4906634, 4775757, 4727072, 4542160,
 4522949, 4524151, 4525479, 4474804, 4520026, 4520026, 5869478, 5859239,
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 25 5414013, 5401758, 5393771, 5362902, 5332737, 5310731, 5260444, 5223516,
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5 4560698, 4556739, 4556675, 4555571, 4555570, 4555523, 4550120, 4542160,
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3897441, 3886157, 3883540, 3873715, 3867383, 3873715, 3867383, 3691216,
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15 antimicrobial agents as disclosed in U.S. Patent no.'s 5902594, 5874476,
5874436, 5859027, 5856320, 5854242, 5811091, 5786350, 5783177, 5773469,
5762919, 5753715, 5741526, 5709870, 5707990, 5696117, 5684042, 5683709,
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5190961, 5175160, 5157051, 5096700, 5093342, 5089251, 5073570, 5061702,
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3966968, 3954868, 3936393, 3917476, 3915889, 3867548, 3865748, 3867548,
3865748, 3783160, 3764676, 3764677;

30 anti-inflammatory agents as disclosed in U.S. Patent no.'s 5872109,
5837735, 5827837, 5821250, 5814648, 5780026, 5776946, 5760002, 5750543,
5741798, 5739279, 5733939, 5723481, 5716967, 5688949, 5686488, 5686471,
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 5 5324648, 5319099, 5318971, 5312821, 5302597, 5298633, 5298522, 5298498,
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 10 5143929, 5143928, 5143927, 5124455, 5124347, 5114958, 5112846, 5104656,
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 4556669, 4539326, 4537903, 4536503, 4518608, 4514415, 4512990, 4501755,
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 25 4201778, 4181720, 4173650, 4173634, 4145444, 4128664, 4125612, 4124726,
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 30 3726978, 3694471, 3691214, 3678169, 3624216;

immunosuppressive agents, as disclosed in U.S. Patent no.'s 4450159,
 4450159, 5905085, 5883119, 5880280, 5877184, 5874594, 5843452, 5817672,
 5817661, 5817660, 5801193, 5776974, 5763478, 5739169, 5723466, 5719176,
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5484788, 5470857, 5464615, 5432183, 5431896, 5385918, 5349061, 5344925,
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10 4256766, 4180588, 4000275, 3759921;

analgesic agents, as disclosed in U.S. Patent no.'s 5292736, 5688825,
5554789, 5455230, 5292736, 5298522, 5216165, 5438064, 5204365, 5017578,
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4251530, 4244955, 4232018, 4209520, 4164514 4147872, 4133819, 4124713,
4117012, 4064272, 4022836, 3966944;

25 cholinergic agents, as disclosed in U.S. Patent no.'s 5219872, 5219873,
5073560, 5073560, 5346911, 5424301, 5073560, 5219872, 4900748, 4786648,
4798841, 4782071, 4710508, 5482938, 5464842, 5378723, 5346911, 5318978,
5219873, 5219872, 5084281, 5073560, 5002955, 4988710, 4900748, 4798841,
4786648, 4782071, 4745123, 4710508;

30 adrenergic agents, as disclosed in U.S. Patent no.'s 5091528, 5091528,
4835157, 5708015, 5594027, 5580892, 5576332, 5510376, 5482961, 5334601,
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antihistamine agents, as disclosed in U.S. Patent no.'s 5874479, 5863938, 5856364, 5770612, 5702688, 5674912, 5663208, 5658957, 5652274, 5648380, 5
5646190, 5641814, 5633285, 5614561, 5602183, 4923892, 4782058, 4393210, 4180583, 3965257, 3946022, 3931197;

steroidal agents, as disclosed in U.S. Patent no.'s 5863538, 5855907, 5855866, 5780592, 5776427, 5651987, 5346887, 5256408, 5252319, 5209926, 4996335, 4927807, 4910192, 4710495, 4049805, 4004005, 3670079, 3608076, 10
5892028, 5888995, 5883087, 5880115, 5869475, 5866558, 5861390, 5861388, 5854235, 5837698, 5834452, 5830886, 5792758, 5792757, 5763361, 5744462, 5741787, 5741786, 5733899, 5731345, 5723638, 5721226, 5712264, 5712263, 5710144, 5707984, 5705494, 5700793, 5698720, 5698545, 5696106, 5677293, 5674861, 5661141, 5656621, 5646136, 5637691, 5616574, 5614514, 5604215, 15
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30 Also of interest are analogs of the above compounds.

For all of the above active agents, the active agents may be present as pharmaceutically acceptable salts.

As indicated above, the active agent of the compositions are typically present in a pharmaceutically acceptable vehicle or carrier, e.g., as described

below. In certain embodiments, the active agent is present in an amount of from about 0.1% to about 90% by weight, e.g., from about 1% to about 30% by weight of the active compound.

5 Pharmaceutically Acceptable Carrier

As summarized above, the compositions of the invention further include a pharmaceutically acceptable vehicle (i.e., carrier). Common carriers and excipients, such as corn starch or gelatin, lactose, dextrose, sucrose, microcrystalline cellulose, kaolin, mannitol, dicalcium phosphate, sodium chloride,
10 and alginic acid are of interest. Disintegrators commonly used in the formulations of the invention include croscarmellose, microcrystalline cellulose, corn starch, sodium starch glycolate and alginic acid.

A liquid composition may comprise a suspension or solution of the compound or pharmaceutically acceptable salt in a suitable liquid carrier(s), for
15 example, ethanol, glycerine, sorbitol, non-aqueous solvent such as polyethylene glycol, oils or water, with a suspending agent, preservative, surfactant, wetting agent, flavoring or coloring agent. Alternatively, a liquid formulation can be prepared from a reconstitutable powder. For example, a powder containing active compound, suspending agent, sucrose and a sweetener can be reconstituted
20 with water to form a suspension; and a syrup can be prepared from a powder containing active ingredient, sucrose and a sweetener.

A composition in the form of a tablet or pill can be prepared using any suitable pharmaceutical carrier(s) routinely used for preparing solid compositions. Examples of such carriers include magnesium stearate, starch, lactose, sucrose,
25 microcrystalline cellulose and binders, for example, polyvinylpyrrolidone. The tablet can also be provided with a color film coating, or color included as part of the carrier(s). In addition, active compound can be formulated in a controlled release dosage form as a tablet comprising a hydrophilic or hydrophobic matrix.

"Controlled release", "sustained release", and similar terms are used to
30 denote a mode of active agent delivery that occurs when the active agent is released from the delivery vehicle at an ascertainable and controllable rate over a period of time, rather than dispersed immediately upon application or injection. Controlled or sustained release may extend for hours, days or months, and may vary as a function of numerous factors. For the pharmaceutical composition of

the present invention, the rate of release will depend on the type of the excipient selected and the concentration of the excipient in the composition. Another determinant of the rate of release is the rate of hydrolysis of the linkages between and within the units of the polyorthoester. The rate of hydrolysis in turn may be controlled by the composition of the polyorthoester and the number of hydrolysable bonds in the polyorthoester. Other factors determining the rate of release of an active agent from the present pharmaceutical composition include particle size, acidity of the medium (either internal or external to the matrix) and physical and chemical properties of the active agent in the matrix.

A composition in the form of a capsule can be prepared using routine encapsulation procedures, for example, by incorporation of active compound and excipients into a hard gelatin capsule. Alternatively, a semi-solid matrix of active compound and high molecular weight polyethylene glycol can be prepared and filled into a hard gelatin capsule; or a solution of active compound in polyethylene glycol or a suspension in edible oil, for example, liquid paraffin or fractionated coconut oil can be prepared and filled into a soft gelatin capsule.

Tablet binders that can be included are acacia, methylcellulose, sodium carboxymethylcellulose, poly-vinylpyrrolidone (Povidone), hydroxypropyl methylcellulose, sucrose, starch and ethylcellulose. Lubricants that can be used include magnesium stearate or other metallic stearates, stearic acid, silicone fluid, talc, waxes, oils and colloidal silica.

Flavoring agents such as peppermint, oil of wintergreen, cherry flavoring or the like can also be used. Additionally, it may be desirable to add a coloring agent to make the dosage form more attractive in appearance or to help identify the product.

The compounds of the invention and their pharmaceutically acceptable salts that are active when given parenterally can be formulated for intramuscular, intrathecal, or intravenous administration.

A typical composition for intramuscular or intrathecal administration will be of a suspension or solution of active ingredient in an oil, for example, arachis oil or sesame oil. A typical composition for intravenous or intrathecal administration will be a sterile isotonic aqueous solution containing, for example, active ingredient and dextrose or sodium chloride, or a mixture of dextrose and sodium chloride. Other examples are lactated Ringer's injection, lactated Ringer's plus

dextrose injection, Normosol-M and dextrose, Isolyte E, acylated Ringer's injection, and the like. Optionally, a co-solvent, for example, polyethylene glycol, a chelating agent, for example, ethylenediamine tetraacetic acid, and an anti-oxidant, for example, sodium metabisulphite may be included in the formulation.

5 Alternatively, the solution can be freeze dried and then reconstituted with a suitable solvent just prior to administration.

The compounds of the invention and their pharmaceutically acceptable salts which are active on rectal administration can be formulated as suppositories. A typical suppository formulation will generally consist of active
10 ingredient with a binding and/or lubricating agent such as a gelatin or cocoa butter or other low melting vegetable or synthetic wax or fat.

The compounds of this invention and their pharmaceutically acceptable salts which are active on topical administration can be formulated as transdermal compositions or transdermal delivery devices ("patches"). Such compositions
15 include, for example, a backing, active compound reservoir, a control membrane, liner and contact adhesive. Such transdermal patches may be used to provide continuous or discontinuous infusion of the compounds of the present invention in controlled amounts. The construction and use of transdermal patches for the delivery of pharmaceutical agents is well known in the art. For example, see U.S.
20 Pat. No. 5,023,252.

Such patches may be constructed for continuous, pulsatile, or on demand delivery of pharmaceutical agents.

Optionally, the pharmaceutical composition may contain other pharmaceutically acceptable components, such as buffers, surfactants, antioxidants, viscosity modifying agents, preservatives and the like. Each of these
25 components is well-known in the art. For example, see U.S. Pat. No. 5,985,310.

Other components suitable for use in the formulations of the present invention can be found in Remington's Pharmaceutical Sciences, Mace
30 Publishing Company, Philadelphia, Pa., 17th ed. (1985).

Identifiers

Also present in the subject compositions is an identifier. The identifier may vary depending on the particular embodiment and intended application of the

composition. In certain embodiments, the identifier is a component that emits a signal upon activation by a stimulus, e.g., by interrogation, upon contact with a target physiological location, etc. As such, the identifier may be an identifier that emits a signal when it contacts a target body (i.e., physiological) site. In addition
5 or alternatively, the identifier may be an identifier that emits a signal when interrogated.

In yet other embodiments, the identifier is an inert, but identifiable marker, e.g., an engraved identifier (such as one that is fabricated from a material or materials that survive digestion). This marker may then be identified, for example,
10 following an autopsy or forensic examination. It is possible to provide a more internal device within a pill to determine both that its surface has partially been subject to digestion, but also that the inner pill material has also been digested. This application is particularly useful in experimental pharmacological settings. The identifier of these embodiments is one that does not necessarily emit a
15 signal, but which can be optically inspected, e.g., visually or machine read, to obtain information about the composition with which it was associated prior to administration.

While the identifier may be an identifier that does not emit a signal, in certain embodiments (as summarized above) the identifier is one that does emit a
20 signal. Depending on the needs of a particular application, the signal may be a generic signal, e.g., a signal that merely identifies that the composition has contacted the target site, or a unique signal, e.g., a signal which in some way uniquely identifies that a particular composition from a group or plurality of different compositions in a batch has contacted a target physiological site. As
25 such, the identifier may be one that, when employed in a batch of unit dosages, e.g., a batch of tablets, emits a signal which cannot be distinguished from the signal emitted by the identifier of any other unit dosage member of the batch. In yet other embodiments, the identifier emits a signal that uniquely identifies a given unit dosage, even from other identical unit dosages in a given batch.
30 Accordingly, in certain embodiments the identifier emits a unique signal that distinguishes a given type of unit dosage from other types of unit dosages, e.g., a given medication from other types of medications. In certain embodiments, the identifier emits a unique signal that distinguishes a given unit dosage from other unit dosages of a defined population of unit dosages, e.g., a prescription, a batch

or a lifetime production run of dosage formulations. In certain embodiments, the identifier emits a signal that is unique, i.e., distinguishable, from a signal emitted by any other dosage formulation ever produced, where such a signal may be viewed as a universally unique signal (e.g., analogous to a human fingerprint which is distinct from any other fingerprint of any other individual and therefore uniquely identifies an individual on a universal level). In one embodiment, the signal may either directly convey information about the composition, or provide an identifying code, which may be used to retrieve information about the composition from a database, i.e., a database linking identifying codes with compositions.

The identifier may be any component or device that is capable of generating a detectable signal following activation in response to a stimulus. In certain embodiments, the stimulus activates the identifier to emit a signal once the composition comes into contact with a physiological target site, e.g., as summarized above. For example, a patient may ingest a pill that upon contact with the stomach fluids, generates a detectable signal. Depending on the embodiment, the target physiological site or location may vary, where representative target physiological sites of interest include, but are not limited to: a location in the gastrointestinal tract (such as the mouth, esophagus, stomach, small intestine, large intestine, etc.); another location inside the body, such as a parental location, vascular location, etc.; or a topical location; etc.

In certain embodiments the stimulus that activates the identifier is an interrogation signal, such as a scan or other type of interrogation. In these embodiments, the stimulus activates the identifier, thereby emitting a signal which is then received and processed, e.g., to identify the composition in some manner.

In certain of these embodiments, the identifier may include a power source that transduces broadcast power and a signal generating element that modulates the amount of transduced power, such that a signal is not emitted from the identifier but instead the amount of broadcast power transduced by the identifier is detected and employed as the "signal." Such embodiments are useful in a variety of applications, such as applications where the history of a given composition is of interest, e.g., as reviewed in greater detail below.

In certain embodiments, the identifier is dimensioned to be complexed with the active agent/pharmaceutically acceptable carrier component of the

composition so as to produce a composition that can be readily administered to a subject in need thereof. As such, in certain embodiments, the identifier element is dimensioned to have a width ranging from about 0.05 mm to about 1 mm, such as from about 0.1 mm to about 0.2 mm; a length ranging from about 0.05 mm to about 1 mm, such as from about 0.1 mm to about 0.2 mm and a height ranging from about 0.1 mm to about 1 mm, such as from about 0.05 mm to about 0.3 mm, including from about 0.1 mm to about 0.2 mm. In certain embodiments the identifier is 1 mm³ or smaller, such as 0.1 mm³ or smaller, including 0.2 mm³ or smaller. The identifier element may take a variety of different configurations, such as but not limited to: a chip configuration, a cylinder configuration, a spherical configuration, a disc configuration, etc, where a particular configuration may be selected based on intended application, method of manufacture, etc.

The identifier may generate a variety of different types of signals, including but not limited, RF, magnetic, conductive (near field), acoustic, etc.

As is known in the art (see, e.g., J.D. Jackson, *Classical Electrodynamics*, 2nd Edition, pp. 394-396 (1975)), the electric (**E**) and magnetic (**B**) fields for radiation of an oscillating electric dipole antenna with an angular frequency ω and corresponding wave number k (where $k = \omega/c$, with c being the speed of light in the relevant medium) are given by the equations:

$$\mathbf{B} = k^2 (\mathbf{n} \times \mathbf{p}) \frac{e^{ikr}}{r} \left(1 - \frac{1}{ikr} \right); \text{ and} \quad (1)$$

$$\mathbf{E} = k^2 (\mathbf{n} \times \mathbf{p}) \times \mathbf{n} \frac{e^{ikr}}{r} + [3\mathbf{n}(\mathbf{n} \cdot \mathbf{p}) - \mathbf{p}] \left(\frac{1}{r^3} - \frac{ik}{r^2} \right) e^{ikr}, \quad (2)$$

where $\mathbf{n}$ is a unit vector in the direction from the center of the dipole source to a location $\mathbf{x}$ at a distance r from the source, and $\mathbf{p}$ is a space-integrated density of electric charge given by $\mathbf{p} = \int \mathbf{x}' \rho(\mathbf{x}') d^3x'$.

As can be seen from Eqs. (1) and (2), in the "far field" region, where $r \gg \lambda$ (where the wavelength $\lambda = 2\pi/k$), the electric and magnetic fields are dominated by terms that decrease with distance as $1/r$. In this region, mutually perpendicular electric and magnetic fields feed off one another to propagate the signal through space. Where $\lambda \sim r$, the $1/r^2$ ("induction") terms in Eqs. (1) and (2) become significant, and where $\lambda \gg r$, an additional quasi-electrostatic term that varies as $1/r^3$ also becomes significant.

Conventional RF communication takes place at distances $r \sim \lambda$ to $r \gg \lambda$. For instance, implantable medical devices such as pacemakers typically communicate in the 405-MHz frequency band, corresponding to wavelengths of 0.75 meters, somewhat smaller than the scale of a human body. As is known in the art, higher frequencies are advantageously not used because structures within the body begin to absorb radiation, leading to undesirable signal loss; substantially lower frequencies (longer wavelengths) are generally regarded as undesirable because much of the energy is redirected into the induction and/or quasi-static field components rather than the far-field component that can be sensed using conventional antennas. It should also be noted that RFID applications with a transponder and a base unit typically use wavelengths such that $r \sim \lambda$ and generally rely on magnetic induction to transmit power from the transponder to the base unit. In certain embodiments, these RF signals are employed.

In contrast to these approaches, certain embodiments of the present invention advantageously operate at wavelengths much larger than the human body ($\lambda \gg 1$ meter) to communicate information within the patient's body.

For instance, in some embodiments, frequencies on the order of 100 kHz, corresponding to wavelengths of around 3 km (in air), are advantageously used. At distances r that are short as compared to the wavelength λ , the quasi-static electric field term in Eqs. (1) and (2) dominates, and thus the propagating signal is predominantly electrical rather than electromagnetic. Such signals readily propagate in a conductive medium such as the human body. For instance, at a frequency of 100 kHz and distances on the order of 1-2 meters, the quasi-static ($1/r^3$) component of Eq. (2) is estimated to be on the order of 10^6 times stronger than the far-field ($1/r$) component. Thus, long-wavelength signaling using near-field coupling is efficient. Further, because the signals are required to travel relatively short distances (typically 2 meters or less), detectable signals can be transmitted using very small antennas.

A wide range of frequencies may be used for transmission of signals. In some embodiments, the transmission frequency is within the "LF" band (low frequency, defined as 30-300 kHz) of the RF spectrum, below the frequency

range of AM radio (around 500 to 1700 kHz). Within the LF band, the range from 160-190 kHz has been designated by the FCC for experimental use, with specified upper limits on external signal strength. In embodiments of the present invention where the signals are largely confined within the patient's body as
5 described below, this experimental band can be used.

However, the invention is not limited to the 160-190 kHz band or to the LF (30-300 kHz band). Lower bands may also be used; for instance, in the VLF band (3-30 kHz, wavelengths of 10-100 km in air), signals can penetrate water to a distance of 10-40 meters. Since the electrical properties of the human body are
10 similar to those of salt water, it is expected that signals in this band would also readily propagate through the body. Thus, any frequency band corresponding to a wavelength that is at least an order of magnitude larger than the human body — e.g., $\lambda \sim 10$ m or longer, or frequencies on the order of 30 MHz or below — can be used.

15 While there is no necessary lower limit on the frequency of signals used, several practical considerations may affect the choice of frequency. For instance, it is well known that the human body carries low-level oscillating signals induced by nearby AC-powered devices, which operate at 60 Hz (US) or similar frequencies in other parts of the world. To avoid interference caused by AC
20 electrical power systems, frequencies near 60 Hz are advantageously not used. In addition, as is known in the art, longer wavelengths correlate with lower information transfer rates, and the information-transfer capacity at long wavelengths (e.g., below the 3 kHz-30kHz VLF band) may be too small for the amount of information that is to be transferred in a particular system. Further,
25 longer wavelengths generally require longer dipole antennas to produce a detectable signal, and at some point the antenna size may become a limiting factor in frequency selection.

According to some embodiments of the invention, given a suitable choice of frequency, a signal strong enough to travel to a receiver within the body can be
30 generated using a very small antenna. For instance, 100 kHz signals generated by a dipole antenna just a few millimeters long can be propagated to a receiver antenna placed 1-2 meters away. This quasi-electrostatic transmission is believed to be aided by the fact that the implanted antenna is directly in contact

with a conductive medium, for example, the patient's tissues. For purposes of analyzing electrical properties, human tissue can be approximated as an electrolyte solution with electrical properties comparable to those of salt water. Thus, as in an electrolyte bath, the quasi-electrostatic field created by an oscillating dipole antenna induces an oscillating current in the body. As a result of the inherent electrical resistivity of the body (comparable to salt water), the oscillating current creates oscillating potential variations within the body that can be sensed using a suitable receiver. (See, e.g., L.D. Landau et al. *Electrodynamics of Continuous Media*, Ch. 3 (1960)). Examples of suitable receivers include the leads of a pacemaker, which create a dipole with an axis of about 20 cm or any other implanted wires with length from 10-100 cm.

It should be noted that these currents are undesirable in the context of conventional RF communication, in which current flow in the near field leads to power loss in the far-field. In fact, many RF transmitters include devices designed to minimize near-field current leakage. In near-field transmitters of these embodiments of the present invention, maximizing such currents is desirable.

Further, for quasi-electrostatic signals, the patient's skin advantageously acts as a conductive barrier, confining the signals within the patient's body. This confines the signals within the body and also makes it difficult for stray external signals to penetrate the body and create noise or interference in the transmitted signals. Confinement of the signals can mitigate, to some extent, the $1/r^3$ falloff of the near-field signal, further reducing power requirements. Such effects have been observed in the laboratory, e.g., in a salt water bath, in which the water/air interface acting as a conductive barrier. Similar effects have been observed in communicating with submarines via RF transmission in the ELF (3-30Hz) and SLF (30-300 Hz) bands. These effects have also been observed in sonar communications; although sonar uses acoustic, rather than electrical or electromagnetic, fields to transmit information, the surface of the water acts as a conductive barrier for acoustic energy and mitigates the fall-off of signal intensity with distance.

As a result of these phenomena, a transmitter with a very small antenna and a small power source are sufficient to create a near-field signal that is detectable within the patient's body. For instance, the antenna can be formed by

a pair of electrodes a few millimeters or less in length, spaced apart by a few millimeters, with oscillating voltages of opposite phase applied to create an oscillating electric dipole. Such antennas can be disposed almost anywhere within the body.

5 Further, in some embodiments, the frequency, transmitter antenna length, and receiver antenna length are selected such that only microwatts of power are required to produce a detectable signal, where conventional RF communication (e.g., at around 405 MHz) would require at least milliwatts. Accordingly, very compact power supplies that produce only small amounts of
10 power can be used; examples are described in Section IV below.

As such, depending on the particular embodiment of interest, the frequency may range from about .1 Hz or lower to about 100 mHz or higher, e.g., from about 1 kHz to about 70 mHz, including from about 5 kHz to about 200 kHz.

In certain embodiment, the signal that is emitted by the identifier is an
15 acoustic signal. In these embodiments, any convenient acoustic signal generation element may be present in the identifier, e.g., a piezoelectric element, etc.

The transmission time of the identifier may vary, where in certain embodiments the transmission time may range from about 0.1 μ sec to about 4 hours or longer, such as from about 1 sec to about 4 hours. Depending on the
20 given embodiment, the identifier may transmit a signal once or transmit a signal two or more times, such that the signal may be viewed as a redundant signal.

In certain embodiments, the identifier may be one that is programmable following manufacture, in the sense that the signal generated by the identifier may be determined after the identifier is produced, where the identifier may be
25 field programmable, mass programmable, fuse programmable, and even reprogrammable. Such embodiments are of interest where uncoded identifiers are first produced and following incorporation into a composition are then coded to emit an identifying signal for that composition. Any convenient programming technology may be employed. In certain embodiments, the programming
30 technology employed is RFID technology. RFID smart tag technology of interest that may be employed in the subject identifiers includes, but is not limited to: that described in U.S. Patent Nos. 7,035,877; 7,035,818; 7,032,822; 7,031,946, as well as published application no. 20050131281, and the like.

With RFID or other smart tag technology, a manufacturer/vendor may associate a unique ID code with a given identifier, even after the identifier has been incorporated into the composition. In certain embodiments, each individual or entity involved in the handling of the composition prior to use may introduce information into the identifier, e.g., in the form of programming with respect to the signal emitted by the identifier, e.g., as described in U.S. Patent No. 7,031,946.

The identifier of certain embodiments includes a memory element, where the memory element may vary with respect to its capacity. In certain embodiments, the memory element has a capacity ranging from about 1 bit to 1 gigabyte or more, such as 1 bit to 1 megabyte, including from about 1 bit to about 128 bit. The particular capacity employed may vary depending on the application, e.g., whether the signal is a generic signal or coded signal, and where the signal may or may not be annotated with some additional information, e.g., name of active agent, etc.

Identifier components of embodiments of the invention have: (a) an activation component and (b) a signal generation component, where the signal generation component is activated by the activation component to produce an identifying signal, e.g., as described above.

Activation Component

The activation component is a component that activates the signal generation element to emit a signal upon experience of a stimulus, e.g., contact of the composition with a target physiological site of interest, such as the stomach. The activation component may be configured to be activated in a number of different ways. The following sections detail certain different ways in which the identifier may be activated. As can be seen from the following review, the activation component may or may not be integrated with a power source, e.g., a battery. Illustrative activation approaches include, but are not limited to: Battery Completion, e.g., Battery activated by electrolyte addition and Battery activated by cathode or anode addition; Battery connection, e.g., Battery activated by conductor addition; Transistor-mediated Battery Connection, e.g., Battery activated by transistor gate, Geometry Modification, Detection of Geometry

Modification by Resonant Structure, Pressure Detection, Resonant Structure Modification; etc. Each of these illustrative activation approaches is now reviewed in greater detail.

Battery Completion

5 Battery activated by electrolyte addition

In these embodiments, the battery includes, when completed, a cathode, an anode, and an electrolyte. When the composition (e.g., pill) is administered, e.g., ingested, and travels through the esophagus, it proceeds to enter the stomach. The cathode and anode provided within the composition do not
10 constitute a full battery. However, as the composition dissolves to expose the cathode and anode, the stomach fluid acts as the electrolyte component of the battery. The added component of the stomach fluid thus completes the battery. Therefore, as the composition contacts the target site, e.g., by entering the stomach and dissolving to the point of cathode and anode exposure, a power
15 source is provided which activates the identifier, e.g., in chip configuration. The data signal is then transmitted. This configuration is described in greater detail below, e.g., in terms **FIG. 4**.

Battery activated by cathode or anode addition

In an extension of this approach, the system is activated by having the
20 triggering event add a cathode or anode component, with the electrolyte being intrinsic in the partial, pre-battery configuration. The battery is completed, producing power and activating the composition, although not necessarily at the identical point of time.

25 Battery connection

Battery activated by conductor addition

In another embodiment of the present invention, the battery is connected to the circuitry when it enters the stomach. The battery becomes connected, and thus activates the identifier, by conductor addition. In this case, there is a
30 physically complete battery and a complete chip. When these two components are awash in physiological fluid, such as in the stomach, they become electronically connected. This triggering event electrically connects the battery to the signaling microchip, thus activating the smart pill.

Transistor-mediated Battery Connection

Battery activated by transistor gate

Another design allowing the battery and the chip together to activate the smart pill has the feature of a transistor gate between the battery and the reporting chip. Once the transistor gate is switched on, such as by activation with
5 the stomach, the reporting signal is transmitted.

There are numerous methods well known to the ordinary skilled artisan for turning on a transistor gate. Most of them involve activating the gate by closing a switch, which can include a transistor switch or other types of switches.

The gate can be activated by applying a small gate current. This is how,
10 for example, transistors are typically activated. The gate current can be generated in any number of ways well known to the ordinary skilled artisan. Any circuitry which detects the presence of the pill in the environment of interest, such as the stomach, generates the gate current and turns the system on.

The gate current can be turned on by detecting a conductivity variation.
15 For instance, a circuit can be provided that detects a small change in the conductivity of the stomach. While the stomach is conductive, the pill might not be. As a result, when the conductivity variation is detected, the transistor gate is activated, turning the smart pill on and generating a reporting signal.

The conductivity can be modulated by a change in the solution
20 concentration. By example, the system detects a different solution concentration in the stomach in contrast to areas outside the stomach. The solution pH is detected, by a modulation of the conductivity, which turns on the gate, and turn on the pill generating a reporting signal.

The stomach contains ionic conductive fluids. Those ionic conductive
25 fluids can be employed to modulate the conductivity of the gate and turn on the smart pill, generating a reporting signal. Individual enzymes can be detected in the stomach. For instance, a chem-FET can be employed that looks for the pepsin content in the stomach, turning the pill on, thus reporting the presence of the enzyme.

30 Temperature change can also be detected using the innovations of the present invention. The stomach is typically a steady 37°C. Areas outside the stomach are more typically 20°C or less. When the pill enters the stomach and becomes heated up, the pill is so designed that this adjusts the conductivity and turn the identifier on, generating a reporting signal.

The conductivity of the transistor can be modified by a microscopic property called carrier mobility. A detection approach using this property uses the transistor itself as a detector. The carrier mobility is modulated by temperature, a well-known phenomenon. In this manner, the transistor is used
5 as a temperature sensor by using that transistor to turn on the smart pill, generating a reporting signal.

Another approach is to change the charge on the gate of a MOSFET transistor. The gate charge can be modulated by the factors to be detected. This is again a configuration using the transistor to turn on the circuit, generating a
10 reporting signal.

In another configuration, the gate charge is modulated by a material to be detected in the solution. A specific ion would preferentially change the gate charge. This system is modulated by a crystal potential. A crystal potential occurs when crystals generate electric fields under certain circumstances.

15 The electric field can change the charge on the gate, turning on the transistor and generating a reporting signal. This change may be modulated by a chemical potential, resulting from an osmotic or ionic process. This causes charge to accumulate on the gate, thereby, turning it on and generating a reporting signal.

20 A change in the electrical potential can also cause a reporting signal using a variety potentials. For example, a gravitational potential can detect the change in height of the detector. In the case of a patient swallowing the pill, the change in pill height would indicate ingestion.

In another embodiment, a transistor gate has associated with it a
25 capacitance. That capacitance is then modulated by certain properties peculiar to the target site, e.g., the stomach.

In one case, the capacitance is changed by being enveloped in the stomach. This effect on the capacitance is then detected. The gate charge is modulated by change in the carrier concentration. The carrier concentration is
30 modulated by temperature. This approach provides a slightly different approach, but similar in concept to using the transistor as a temperature sensor as above.

Geometry Modification

A transistor structure is also provided that has a geometry that changes. Gate capacitance is determined by a change in geometry which occurs in the

stomach, detecting a change in capacitance. These changes can take place in a variety of ways, for example, as further described below.

A variety of physiologic factors change the geometry. Pressure in the stomach different than pressure outside occurs with the natural squeezing during the production of chyme, as well as at other times. This changes the gate capacitance. The change is detected by having a dielectric on the gate. In this case, the gate consists of a number of layers, one of which is the dielectric.

In an additional embodiment, the enzymes of the stomach dissolve the dielectric, changing the gate capacitance, which is then detected. Various physical and chemical conditions within the stomach dissolve that gate dielectric, thereby activating the circuit.

Detection of Geometry Modification by Resonant Structure

A resonant structure on the gate is provided in other variants. In this case, a mechanical structure is provided that has a characteristic frequency. This frequency is excited by the triggering event, and measured. Various interactions with the stomach will cause a change in that resonance.

Pressure Detection

Gate capacitance and resonance with modulation source can also be utilized for detection. In this case, an excitation is provided to the resonance structure from a modulation source, such as a sound wave. The gate capacitance of that resonance structure can be used to detecting pressure waves. A resonance structure sits out in the stomach and is hooked up to a detection circuit on a transistor. In the stomach, the resonance circuit detects pressure waves.

Of pressure sound waves within the body, there are particular sounds that are characteristic, such as the heart beat and respiration. These sounds are detected and used to turn the circuit on.

Pressure waves are also detected by resonant Q factor modulation. Q factor modulation can be accomplished in a number of different manners. The resonance structure has two components, a frequency and a Q factor. The Q factor is modulated by detecting some environmental change.

Resonant Structure Modification

By example, the structure has a very different Q factor in air than it does in the fluid of the stomach. Thus, the dampening can be detected by the fluid

viscosity. Additionally, the structure can be configured to be eaten away by the acid or some of the enzymes in the stomach, which changes the cue.

Degradation by stomach acid or enzymes also changes the resonant frequency. It is simple to detect the frequency shift of such a structure. The frequency is shifted as this structure is changed in the stomach. There are two approaches to modifying the structure. A catabolic process can occur where the structure gets dissolved, which is easily detectable. Also, an anabolic process would occur where an enzyme from the stomach binds to this structure, making it larger. This effect will also modify the resonance structure. The resonance modification is detected either as a frequency change or a Q factor modulation.

Battery Power Sources

As reviewed above, in certain embodiments, the activation element is a power source that is turned on upon contact of the power source with a target site, e.g., a physiological target site, such as the stomach, e.g., stomach acid. In certain embodiments, the power source is a battery that is turned on to provide power upon contact with the physiological target site, where the battery is coupled to the signal generation component such that when the battery is turned on, the signal generation component emits the identifying signal.

In certain embodiments, the battery that is employed is one that comprises two dissimilar materials which constitute the two electrodes of the battery. In certain embodiments, these two materials are shielded from the surrounding environment by an additional layer of material. When the shielding material (e.g., active agent/carrier matrix), is dissolved or eroded by the surrounding fluid, the electrode materials are exposed and come in contact with the body fluid, such as stomach acid or other types of electrolyte fluid. A potential difference, that is, a voltage, is generated between the electrodes as a result of the respective oxidation and reduction reactions incurred to the two electrode materials. A voltaic cell, or battery, can be thereby formed. Accordingly, in embodiments of the invention, such batteries are configured such that when the two dissimilar materials are exposed to the target site, e.g., the stomach, the digestive tract, etc., during the physical and chemical erosion of the composition in which the signal generation element is present, a voltage is generated. In such embodiments, the power source described above is not a "battery" in the

common sense of the word, but rather as defined in the discipline of physics. The two dissimilar materials in an electrolyte are at different potentials, similar to the physics model of a 'potato battery'. As an example, copper and zinc when put into a cell have different potentials. Similarly, gold and magnesium have different potentials. As a result, a potential difference between the two dissimilar materials is generated.

Various battery-activation configurations are possible. Representative types of cell-activation approaches include, but are not limited to: activation by presence of electrolyte, activation by presence of a cathode material, activation by presence of a conductive material.

After the battery is activated, further activation configurations can be employed to activate the signal generation component. For example, the signal generation component can be activated through the activation of the gate of a metal oxide semiconductor (MOS) circuit, such as a CMOS switch. Activation of the gate of the MOS circuit can be based on one or more parameters, which include but are not limited to: gate current, gate charge, and gate capacitance.

The gate current, for activation purposes, can be a function of the conductivity of surrounding body fluids or tissues. Such conductivity can further be a function of one or more parameters, which include but are not limited to: solution concentration, solution pH value, ionic content of solution, enzymatic content of solution, temperature, and carrier mobility. Carrier mobility can also be a function of temperature.

Similarly, the gate charge can be a function of one or more parameters, which include but are not limited to: solution composition, crystal potential, electrical potential, gravitational potential, gate capacitance, and carrier concentration. The carrier concentration can also be a function of temperature.

The gate capacitance can be a function of the capacitive geometry of the gate, which can further be a function of pressure, a resonant input, or the characteristics of a dielectric material coupled to the gate. The characteristics of the dielectric material can vary with one or more parameters, which include but are not limited to: chemical contents of a digestive tract, chemical character of a physiological location, and amount of dissolution of the dielectric material in body fluids.

In certain embodiments, the battery is one that is made up of active electrode materials, electrolyte, and inactive materials, such as current collectors, packaging, etc. The active materials are any pair of materials with different electrochemical potentials. Suitable materials are not restricted to metals, and in certain embodiments the paired materials are chosen from metals and non-metals, e.g., a pair made up of a metal (such as Mg) and a salt (such as CuI). With respect to the active electrode materials, any pairing of substances – metals, salts, or intercalation compounds - with suitably different electrochemical potentials (voltage) and low interfacial resistance are suitable.

A variety of different materials may be employed as the battery electrodes. In certain embodiments, electrode materials are chosen to provide for a voltage upon contact with the target physiological site, e.g., the stomach, sufficient to drive the signal generation element of the identifier. In certain embodiments, the voltage provided by the electrode materials upon contact of the metals of the power source with the target physiological site is 0.001 V or higher, including 0.01 V or higher, such as 0.1 V or higher, e.g., 0.3 V or higher, including 0.5 volts or higher, and including 1.0 volts or higher, where in certain embodiments, the voltage ranges from about 0.001 to about 10 volts, such as from about 0.01 to about 10 V.

Materials and pairings of interest include, but are not limited to those reported in Table 1 below.

TABLE 1		
	Anode	Cathode
Metals	Magnesium, Zinc Sodium (†), Lithium (†) Iron	
Salts		Copper salts: iodide, chloride, bromide, sulfate, formate, (other anions possible) Fe ³⁺ salts: e.g. orthophosphate, pyrophosphate, (other anions possible) Oxygen (††) on platinum, gold or other catalytic surfaces
Intercalation compounds	Graphite with Li, K, Ca, Na, Mg	Vanadium oxide Manganese oxide

† Protected anodes: certain high energy anode material such as Li, Na, and other alkali metals are unstable in their pure form in the presence of water or oxygen. These may however be used in an aqueous environment if stabilized. One example of this stabilization is the so-called "protected lithium anode" developed by Polyplus Corporation (Berkeley, CA), where a polymer film is deposited on the surface of lithium metal to protect it from rapid oxidation and allow its use in aqueous environment or air ambient. (Polyplus has IP pending on this).

†† Dissolved oxygen can also serve as a cathode. In this case, the dissolved oxygen in the bodily fluids would be reduced to OH⁻ at a suitable catalytic surface such as Pt or gold. Other catalysts are also possible.

In certain embodiments, one or both of the metals may be doped with a non-metal, e.g., to enhance the voltage output of the battery. Non-metals that may be used as doping agents in certain embodiments include, but are not limited to: sulfur, iodine and the like.

In certain embodiments, the electrode materials are copper iodine (CuI) as the anode and magnesium (Mg) as the cathode. Embodiments of the present invention use electrode materials that are not harmful to the human body.

In certain embodiments, the batteries have a small form factor. Batteries may be 10 mm³ or smaller, such as 1.0 mm³ or smaller, including 0.1 mm³ or smaller, including 0.02 mm³ or smaller. As such, in certain embodiments, the battery element is dimensioned to have a width ranging from about 0.05 mm to about 1 mm, such as from about 0.1 mm to about 0.2 mm; a length ranging from about 0.05 mm to about 1 mm, such as from about 0.1 mm to about 0.2 mm and a height ranging from about 0.1 mm to about 1 mm, such as from about 0.05 mm to about 0.3 mm, including from about 0.1 mm to about 0.2 mm.

As reviewed below, in certain embodiments the battery has a split or segmented configuration.

In certain embodiments, the battery is one which is free of packaging. As such, the electrodes are exposed and not protected by any protecting or sealing structure. As such, following removal of the active agent/carrier matrix material with which the battery may be associated, the battery per se does not itself include any protective packaging such that the electrodes are free to contact the electrolyte at the target physiological location.

In certain of these embodiments, the battery power source may be viewed as a power source that exploits reverse electrolysis in an ionic solution such as gastric fluid, blood, or other bodily fluids and some tissues. FIG. 4 illustrates an identifier 30 having a signal generation element 40 powered by reverse

electrolysis. Signal generation element **40** is electrically connected to metal electrodes **32** and **33**, which are made of two different materials and are electrically insulated from each other. When metal electrodes **32** and **33** are immersed in an ionic solution **39**, a potential difference develops between them; for instance, electrode **33** rises to a higher potential $V+$ while electrode **32** falls to a lower potential $V-$. This potential difference can be used to power circuitry **40**.

Electrodes **32** and **33** can be implemented in various ways; for instance, areas on opposing surfaces of an integrated circuit chip can be coated with two different metals, and the entire chip can be placed in the ionic solution. Alternatively, electrodes **32** and **33** may extend away from element **40** as shown. Other arrangements may also be used.

As illustrated above, electrodes **32** and **33** can be made of any two materials appropriate to the environment in which the identifier **30** will be operating. For instance, in some embodiments where ionic solution **39** comprises stomach acids, electrodes **32** and **33** may be made of a noble metal (e.g., gold, silver, platinum, palladium or the like) so that they do not corrode prematurely. Alternatively, the electrodes can be fabricated of aluminum or any other conductive material whose survival time in the applicable ionic solution is long enough to allow identifier **30** to perform its intended function.

Where the power source is a battery, the battery may be fabricated in a number of different ways. In certain embodiments, fabrication protocols which may be categorized as "planar" processing protocols are employed, as developed in greater detail below.

Additional Power Sources

Other sources, internal or external to the remote device, may also be employed in addition to or instead of those described above. For example, chemical or radioisotope batteries with a suitable form factor may be used to power some remote devices. Recently-developed fuel cells that use blood as an energy source can be miniaturized and used to provide electrical energy for a low-power microchip. Piezoelectric crystals that convert mechanical energy (e.g., compression) to electrical energy can be employed for remote devices disposed where suitable mechanical forces can be brought to bear, such as in or around the heart, stomach, joints, or other moving parts of the body. In yet other

embodiments, a power source modeled on the cellular energy factory, with power being extracted from ATP in the blood so that blood, in effect, "nourishes" the identifier, is employed. In other embodiments, acoustic energy (e.g., ultrasound) can be coupled into a remote device through piezoelectric or similar converters.

5 In yet other embodiments, the activation element is not an on board power source, but an element that is powered from a separate power source and provides an activation signal to the signal generation component upon contact of the composition with the target site. For example, the activation element may be coupled to a power receiver which is configured to receive broadcast power and
10 transduce the broadcast power into a form suitable for driving the signal generation element. In certain embodiments, the power receiver may be a coil. Alternatively, the activator component may be powered by a distinct power source, e.g., a sealed battery, a power element that converts mechanical energy of the pill into electrical power, e.g., a piezoelectric power element, etc. As such,
15 the activator may or may not itself be the power source, and in those embodiments where it is not the power source, the identifier may include a distinct power source, such as receiver or power generator.

Signal Generation Component

20 The signal generation component of the identifier element is a structure that, upon activation by the activation component, emits a detectable signal, e.g., that can be received by a receiver, e.g., as described in greater detail below. The signal generation component of certain embodiments can be any convenient device that is capable of producing a detectable signal and/or modulating
25 transduced broadcast power, upon activation by the activation component. Detectable signals of interest include, but are not limited to: conductive signals, acoustic signals, etc. As reviewed above, the signals emitted by the signal generator may be generic or unique signals, where representative types of signals of interest include, but are not limited to: frequency shift coded signals;
30 amplitude modulation signals; frequency modulation signals; etc.

In certain embodiments, the signal generation element includes circuitry, as developed in more detail below, which produces or generates the signal. The type of circuitry chosen may depend, at least in part, on the driving power that is supplied by the power source of the identifier. For example, where the driving

power is 1.2 volts or above, standard CMOS circuitry may be employed. In other embodiments where the driving power ranges from about 0.7 to about 1.2 V, sub-threshold circuit designs may be employed. For driving powers of about 0.7 V or less, zero-threshold transistor designs may be employed.

5 In certain embodiments, the signal generation component includes a voltage-controlled oscillator (VCO) that can generate a digital clock signal in response to activation by the activation component. The VCO can be controlled by a digital circuit, which is assigned an address and which can control the VCO with a control voltage. This digital control circuit can be embedded onto a
10 chip that includes the activation component and oscillator. Using amplitude modulation or phase shift keying to encode the address, an identifying signal is transmitted.

The signal generation component may include a distinct transmitter component that serves to transmit the generated signal to a remote receiver,
15 which may be internal or external to the patient, as reviewed in greater detail below. The transmitter component, when present, may take a number of different configurations, e.g., depending on the type of signal that is generated and is to be emitted. In certain embodiments, the transmitter component is made up of one or more electrodes. In certain embodiments, the transmitter component is made up
20 of one or more wires, e.g., in the form of antenna(e). In certain embodiments, the transmitter component is made up of one or more coils. As such, the signal transmitter may include a variety of different transmitters, e.g., electrodes, antennas (e.g., in the form of wires) coils, etc. In certain embodiments, the signal is transmitted either by one or two electrodes or by one or two wires. A two-
25 electrode transmitter is a dipole; a one electrode transmitter forms a monopole. In certain embodiments, the transmitter only requires one diode drop of power.

In some embodiments, the transmitter unit uses an electric dipole or electric monopole antenna to transmit signals. **FIG. 6A** illustrates a dipole antenna. Oscillator **504** provides driving signals (ϕ and an inverted signal
30 denoted herein as $/\phi$) to an electrode driver **506**. **FIG. 6C** is a circuit diagram showing details of a dipole electrode driver **600** implemented using conventional CMOS driver circuits. Electrode **602** is driven to a potential E_0 by transistors **604**, **606** in response to driving signal ϕ while electrode **608** is driven to a potential E_1

by transistors **610**, **612** in response to inverted driving signal $/\phi$. Since driving signals ϕ and $/\phi$ oscillate with opposite phase, potentials E_0 and E_1 also oscillate with opposite phase. It will be appreciated that driver **600** and all other electronic circuits described herein can be implemented using sub-micron CMOS processing technologies known in the art; thus, the size of the circuitry is not a limiting factor on the size of a remote device.

In some embodiments, a monopole antenna can be substituted for the dipole antenna of **FIG. 6A**. **FIG. 6D** illustrates a driver circuit for a monopole antenna that can be implemented in conventional CMOS integrated circuits. This antenna driver is generally similar to one half of the driver circuit of **FIG. 6C**, with driver transistors **702**, **704** driving a single electrode **706** to a potential E_m in response to driving signal ϕ .

In either the dipole or monopole case, the driver circuit is powered by a potential difference (ΔV) between terminals $V+$ and $V-$. This potential difference, which can be constant or variable, as desired.

FIG. 6A is a block diagram of a transmitter signal generation element **500** for an identifier according to an embodiment of the present invention. In this embodiment, generation element **500** receives a signal M from the activation component which activates the signal generation element to produce and emit a signal. Signal generation element **500** includes control logic **502**, an oscillator **504**, an electrode driver **506**, and an antenna **508** (in this instance, a pair of electrodes operated as an electric dipole antenna). In operation, oscillator **504** generates an oscillating signal (waveform) in response to signals from control logic **502**. The signals from control logic **502** can start or stop the oscillator and in some embodiments can also shape one or more aspects of the oscillatory signal such as amplitude, frequency, and/or phase. Oscillator **504** provides the waveform to electrode driver **506**, which drives current or voltage on antenna **508** to transmit a signal into the conductive medium of body tissues or fluids.

Depending on a given embodiment, the signal may or may not be modulated. For example, in certain embodiments the frequency of the signal may be held constant. In yet other embodiments, the signal may be modulated in some manner, e.g., via carrier based modulate schemes, ultra-wide band (or time domain based) modulation schemes, etc.

Referring again to **FIG. 6A**, in some embodiments, oscillator **504** operates at a constant frequency. The receipt of a constant-frequency signal in and of itself can provide useful information, e.g., that a remote device is present and operational. In some embodiments, oscillator **504** modulates its signal to
5 encode additional information.

Information can be encoded in various ways, generally by modulating (varying) some property of the transmitted signal, such as frequency, amplitude, phase, or any combination thereof. Modulation techniques known in the art may be employed.

10 In general, information can be transmitted using analog or digital techniques. "Analog techniques" refers generally to instances in which the modulated property is varied in different degrees, with the degree of variation being correlated to a value representing the information to be transmitted. For instance, suppose that element **500** is transmitting a signal. Oscillator **504** can
15 be designed to operate over some range of frequencies. "Digital techniques" refers generally to instances in which the information to be transmitted is represented as a sequence of binary digits (bits), and the signal is modulated based on the bit stream. For instance, suppose again that transmitter **500** is transmitting a signal using digital techniques. Oscillator **504** can be designed to
20 operate at at least two different frequencies, with one frequency corresponding to bit value 0 and another frequency corresponding to bit value 1. In embodiments of the present invention, either analog techniques, digital techniques, or a combination thereof can be used to transmit information. In addition, various types of modulation may be implemented.

25 For instance, in one embodiment, frequency modulation is used. Oscillator **504** can be a voltage-controlled oscillator (VCO), an oscillator circuit in which the oscillation frequency depends on an applied voltage. Control logic **502** supplies an appropriate voltage (e.g., reflecting the value of the measurement data, M), and the frequency of the signal indicates the value of the data. In
30 another embodiment, amplitude modulation is used; for instance, the amplitude of the driving signals ϕ and $1/\phi$ can be varied, or the positive and negative rails of the driver circuit (e.g., $V+$ and $V-$) can be varied to control the amplitude. In another embodiment, phase modulation is used. For instance, in digital signal

transmission, one phase corresponds to bit value 0, an opposite phase corresponds to bit value 1, and the phase shifts represent transitions. Oscillator 504 can include a switch circuit that either directly connects or cross-connects the driving signals ϕ and $/\phi$ to the inputs of a driver circuit. Combinations of frequency modulation, amplitude modulation, and/or phase modulation may also be used as desired.

In some embodiments, the transmitter may transmit a "packet" that includes a unique identifier for the identifier, which in turn is for the composition with which the identifier is associated. The unique identifier may also provide information from the remote device (e.g., the identity of the active agent (i.e., annotation information)). Other techniques for distinguishing different signals may also be used, including: operating different transmitters in different frequency bands, allowing each transmitter to be identified by its frequency and/or configuring different transmitters to transmit at different (and known) times, allowing the transmitter to be identified by when it transmits.

Additional Components

Depending on the particular embodiment, the identifier may include a number of different additional components. Some components of interest include, but are not limited, those reviewed below.

Power Enhancers

Where the activator is a power source that is turned on upon contact with a target physiological site, in certain embodiments, circuits for enhancing or boosting voltage output of the power source, e.g., battery, are provided, e.g., charge pumping circuits, charge doublers, etc. Such voltage enhancing elements may enhance the voltage output by at about 2-fold or more, such as by about 5-fold or more.

Power Storage

In certain embodiments, the activation component includes a power storage element. For example, a duty cycle configuration may be employed, e.g., where slow energy production from a battery is stored in a power storage element, e.g., in a capacitor, which then provides a burst of power that is deployed to the signal generation component. In certain embodiments, the

activation component includes a timing element which modulates, e.g., delays, delivery of power to the signal generation element, e.g., so signals from different compositions, e.g., pills, that are administered at substantially the same time are produced at different times and are therefore distinguishable.

5

Additional Features

In certain embodiments, the compositions are characterized by having one or more of the following features. In certain embodiments, the compositions include an identifier which employs a conductive near-field mode of communication in which the body itself is employed as a conductive medium. In such embodiments, the compositions include circuitry that, when freed from the composition upon disruption of the composition (e.g., as described above) the circuitry comes into direct contact with the body and does not remain encapsulated or protected in some manner. In these embodiments, the signal is not a magnetic signal or high frequency (RF) signal. In certain embodiments, the systems are ones that include a receiver which is stably associated with the body, e.g., implanted or topically applied to an external location, such that the systems are distinguished from those in which an external device that is not stably associated with the body is employed to collect data. In certain embodiments, the compositions do not include an imaging system, e.g., camera or other visualization or imaging element, or components thereof, e.g., CCD element, illumination element, etc. In certain embodiments, the compositions do not include a sensing element, e.g., for sensing a physiological parameter, beyond the activator which detects contact with the targeted physiological site. In certain embodiments, the compositions do not include a propulsion element. In certain embodiments, the compositions do not include a sampling element, such as a fluid retrieval element. In certain embodiments, the compositions do not include an actuatable active agent delivery element, such as an element that retains an active agent with the composition until a signal is received that causes the delivery element to release the active agent.

30

IDENTIFIER FABRICATION

In certain embodiments of interest, the identifier element includes a semiconductor support component. Any of a variety of different protocols may be

employed in manufacturing the identifier structures and components thereof. For example, molding, deposition and material removal, e.g., planar processing techniques, such as Micro-Electro-Mechanical Systems (MEMS) fabrication techniques, including surface micromachining and bulk micromachining techniques, may be employed. Deposition techniques that may be employed in certain embodiments of fabricating the structures include, but are not limited to: electroplating, cathodic arc deposition, plasma spray, sputtering, e-beam evaporation, physical vapor deposition, chemical vapor deposition, plasma enhanced chemical vapor deposition, etc. Material removal techniques included, but are not limited to: reactive ion etching, anisotropic chemical etching, isotropic chemical etching, planarization, e.g., via chemical mechanical polishing, laser ablation, electronic discharge machining (EDM), etc. Also of interest are lithographic protocols. Of interest in certain embodiments is the use of planar processing protocols, in which structures are built up and/or removed from a surface or surfaces of an initially planar substrate using a variety of different material removal and deposition protocols applied to the substrate in a sequential manner.

FIGS. 11A to 13B are diagrams showing a method for fabricating an identifier according to an embodiment of the invention. **Fig. 11A** depicts a cross-section of a semiconductor wafer, **121**, processed by silicon foundry such as IBM or Taiwan Semiconductor Manufacturing Company. The top surface of the wafer, **122**, contains numerous electrical contact pads, **123**, and an insulating dielectric layer, **124**. The contact pads can be Al but could also be Cu, Ti, or similar metal; the dielectric may be a combination of SiO_2 and Si_3N_4 , but could be other insulators. In the first process step, shown in **FIG. 11B**, wafer **121** has been thinned from the back side via grinding or chemical/mechanical polishing to reduce thickness to a desired thickness. A final thickness might be about 300 μm but it can range from about 10 to about 1000 μm such as from about 50 – about 500 μm .

FIG. 12A shows the second process step, in which a layer of corrosion resistant metal, **125**, has been added to the front side of the wafer to cover the electrical contacts, **123**. The typical metal is platinum but one could also use other corrosion resistant metals such as Au, Ti, Ir, or another platinum group

metal. The corrosion resistant metal may be deposited by physical vapor deposition, for example, and may be from about 0.05 to about 100 μm thick, such as from about 0.5 to about 5 μm thick. The metal **125** is formed into a desired pattern via photolithography and etching which are standard semiconductor processing techniques.

FIG. 12B shows the deposition of the cathode material **126**. Cathode materials of interest include, but are not limited to: Cu or CuI, e.g., as described above. They are deposited by physical vapor deposition, electrodeposition, or plasma deposition, among other protocols. The cathode may be from about 0.05 to about 500 μm thick, such as from about 5 to about 100 μm thick. The cathode shape is controlled by shadow mask deposition, or photolithography and etching. Each chip may contain two or more regions, **127** and **127A**, of cathode material as desired.

Next anode material **128A** is deposited as shown in **FIG. 12C**. Anode materials of interest include, but are not limited: Mg, Zn, or other electronegative metals. Adhesion layer **128B** may be necessary to help anode material to adhere to the silicon. Typical adhesion layers for the anode are Ti, TiW, Cr or similar material. Anode material and the adhesion layer may deposited by physical vapor deposition, electrodeposition or plasma deposition. The cathode may be from about 0.05 to about 500 μm thick, such as from about 5 to about 100 μm thick.

FIG. 13A shows the optional protection layer **129A** which is deposited and patterned. In some applications it may be advantageous to control the rate of anode or cathode exposure to the electrolyte environment, so an insulating layer may be deposited and patterned in such a way that it has openings, **129B**, of limited size. This way the solution reaches the anode or cathode material at a controlled rate. **Fig. 13A** illustrates the protection layer on the front (cathode) side of the wafer but it could be also deposited on backside (anode side) of wafer. Typical materials for the protection layer are polyimide, or other photo definable polymer any of which may be spin coated or spray coated. Alternatively a dielectric like SiO_2 , SiC, SiN may be deposited by physical vapor deposition or chemical vapor deposition.

The wafer is then singulated into individual die **115**, **116**, **117** as shown in **FIG. 13B**. Dicing can be accomplished by dicing with a diamond blade saw or by

reactive ion etching. These are standard silicon semiconductor processing techniques. As reviewed above, the chip dimensions may vary. As such, in certain embodiments, the chip (i.e., identifier) element is dimensioned to have a width ranging from about 0.05 mm to about 1 mm, such as from about 0.1 mm to about 0.2 mm; a length ranging from about 0.05 mm to about 1 mm, such as from about 0.1 mm to about 0.2 mm and a height ranging from about 0.1 mm to about 1 mm, such as from about 0.05 mm to about 0.3 mm, including from about 0.1 mm to about 0.2 mm.

10 *SPECIFIC PILL EMBODIMENTS*

In further describing various embodiments of the compositions of the invention, specific embodiments are now described in greater detail in view of the figures. **FIG. 1** provides a diagrammatic, exemplary representation of a pill/capsule embodiment of the present invention, in which the composition is configured as an orally ingestible pharmaceutical formulation in the form of a pill or capsule. The stomach **12** of the patient **10** who ingests the composition **14** is shown. This "smart pill" is shown as it has traveled from the mouth **16** to inside **18** the patient's stomach. Upon reaching the stomach, the pill/capsule undergoes a dissolving process with both the mechanical action of the stomach and the various chemical materials in the stomach fluids, such as hydrochloric acid and other digestive agents.

FIGS. 2A and **2B** provide a more detailed view of the pill composition shown in **FIG. 1**. **FIG. 2A** illustrates an identifier **20** disposed inside a pill **14**. Identifier **20** is present as an integrated circuit (IC). The backside (bottom) of circuit **20** is at least partially coated with a first metal **21**, and a portion of the front (top) of circuit **20** is coated with a different metal **22**, allowing circuit **20** to be powered by reverse electrolysis, e.g., as described above connection with **FIG. 4**. Also on the top surface are two transmitter electrodes **23**, **24**.

When pill **14** is fabricated, the integrated circuit **20** is surrounded by at least one external layer that may include pharmacologically active and/or inert materials in any combination. The external layer dissolves in the stomach through a combination of the mechanical action of the stomach and the action of various chemical constituents (e.g., hydrochloric acid) in stomach fluids.

As pill **14** is dissolved, areas of integrated circuit **20** become exposed to the stomach contents, which for present purposes can be regarded as an electrolyte solution. As dissolution of the pill exposes metal layers **21** and **22**, power is supplied to circuit **20**, which begins to operate and continues to operate
 5 until metal layers **21** and **22** or the circuit itself are sufficiently dissolved by digestive processes and acids to become non-functional. Eventually, the remains of the chip are excreted from the body.

In an alternative embodiment, the integrated circuit **20** is attached to, rather than encapsulated in, the pill **14**. For instance, circuit **20** might be placed
 10 at one end of the pill as the pill is being prepared, in a soluble coating on the surface of the pill, or the like. In embodiments where circuit **20** is wholly or partially exposed, integrated circuit **20** begins to operate sooner after the pill enters the stomach rather than after the pill dissolves.

In one embodiment, circuit **20** transmits a signal identifying pill **14**. The
 15 identifier may indicate the type (active ingredient(s), brand, etc.) and/or dosage of pill **14** and may also provide a lot number, serial number, or similar identifying information that would allow particular pills to be traced, e.g., as reviewed above.

FIG. 2B is a block diagram of one embodiment of electronic circuit **20**. In this embodiment, circuit **20** is a transmitter unit that sequentially transmits a
 20 predetermined series of address (identifier) bits using frequency shift keying, with a first oscillation frequency corresponding to bit value 0 and a second oscillation frequency corresponding to bit value 1. As described above, metal layers **21** and **22** supply power to circuit **20**. The power (not explicitly shown in **FIG. 2B**) is supplied to an oscillator **25**, a counter **26**, a readout circuit **27**, and an electrode
 25 driver **28** that drives transmitter electrodes **29A**, **29B** to transmit the signal. Oscillator **25** may be of generally conventional design (e.g., a ring oscillator) and is advantageously configured to operate in the quasi-electrostatic frequency region as described above. Oscillator **25** generates a driving signal ϕ that oscillates between high and low voltage levels and an inverted driving signal $\bar{\phi}$
 30 that is opposite in phase to driving signal ϕ . In one embodiment, oscillator **25** is a voltage-controlled oscillator (VCO) with an oscillation frequency that depends on a control voltage provided on a signal path **25A**. Counter **26** counts the oscillations of driving signals ϕ and $\bar{\phi}$ and provides the current count to readout

circuit **27**. In one embodiment, counter **26** is an eight-bit counter of generally conventional design; other types of counters (including counters with different widths) may also be used. Readout circuit **27** is configured with a set of address (identifier) bits **27A** that are advantageously fixed, e.g., at the time circuit **20** is fabricated. As noted above, the bits can be unique to a particular instance of pill **14** or common to a lot of pills fabricated under the same conditions or common to all pills containing a particular pharmacological agent. Address bits **14** can be stored in nonvolatile storage circuits of generally conventional design, and any number of address bits (e.g., 8, 16, 32, 48, etc.) may be provided. Readout circuit **27** generates an oscillator control signal (e.g., a voltage) on line **25A** that controls the frequency of VCO **25**. In one embodiment, readout circuit **27** is configured to select a current address bit, e.g., based on the current count provided by counter **26**, and to generate a control signal on signal line **25A** that selects a frequency corresponding to the value of that bit. After some number of cycles (as determined by counter **26**), readout circuit **27** selects the next address bit and generates the corresponding control voltage on signal line **25A**. Various frequencies may be used to represent the address bit values "1" and "0." In one embodiment, frequencies of 100 kHz and 200 kHz may be used to represent values "0" and "1," respectively. Other values (e.g., 1 MHz and 2 MHz or 1 kHz and 5 kHz) may also be used. The chosen frequencies advantageously are well below the absorption modes of human tissues, which are typically above 400 MHz. As described above, VCO **25** generates complementary signals ϕ , $/\phi$ that oscillate at a frequency determined by the control signal on signal line **25A**. The signals ϕ , $/\phi$ are used to control an electrode driver **28**, which may be implemented, e.g., as shown in **FIG. 6D**. It should be noted that since electrodes **21** and **22** are in contact with stomach fluids when circuit **20** is operative, the near-field component is coupled directly into the conductive medium of the patient's body and can be detected by a suitably configured data collector, e.g., as described below. In one embodiment, the collector is configured to log the received address (identifier) and the time of receipt. The data collector can also be configured to retransmit this information to an external device, either in real time or while the patient is in a medical facility. It will be appreciated that the transmitter described herein is illustrative and that variations and modifications

are possible. For instance, other encoding schemes could be used to transmit the data; in one such embodiment, phase shift keying rather than frequency keying is used. In some embodiments, multiple address bits can be encoded into a single symbol that is transmitted using various keying schemes known in the art.

FIG. 3A provides a detailed depiction of an embodiment of a signal generation element **30** which labels the pharmaceutical material and is encapsulated in the center of the composition. Signal generation element **30** is in the form of IC constructed from a silicon chip where various functional elements, e.g., in the form of one or more layers of circuits, are disposed on a silicon substrate **31**. The chip can be fabricated using standard integrated circuit techniques. An example of such a fabrication approach is a 0.5 μ CMOS process made available by AMI Semiconductor in Idaho, USA. Shown on the backside of the substrate, the bottom of the chip **31** is metal 1 **32** which functions as one battery electrode and on the topside of the chip is metal 2 **33** which functions as the other battery electrode. Also on the top side of the chip **31** are electrode 1 **34** and electrode 2 **35**, which constitute a pair of signal-transmission electrodes.

In certain embodiments, electrode 1 **34** and electrode 2 **35** are fabricated from a material that does not readily corrode in the stomach environment, e.g., they are fabricated from noble metals. Alternatively, in some cases the electrodes can be fabricated of a standard aluminum, such as that available from AMI Semiconductor. The criteria for electrode material selection will be readily ascertainable by the ordinary skilled artisan. That is, if the survival time of the electrode is long enough for detection, it is suitable for use. Standard aluminum metals or other lower cost metals if used for electrodes 1 and 2 (**34** and **35**) in appropriate applications allow a lower cost for the device. In some cases dissolution of the electrodes, and thus extinction of the reporting signal, can provide a secondary indication of the full dissolution of the pill and incorporated devices.

Metal 1 and metal 2 (**32** and **33**), in distinction to material selection for the electrode component of the inventive device, are two different metals. Metal 1 and metal 2 are selected so that the potential applied to the silicon is a positive voltage on the top surface and a negative voltage on the bottom surface. In this

way the substrate is essentially at the same potential as the cathode, which can be the ground reference for the circuits, and the top surface, with a SiO₂ insulation layer, is coupled to a positive voltage, referenced to that ground on the bottom side.

5 **FIG. 3B** provides a view of an alternative signal generation element according to an embodiment of the invention. Instead of electrodes, the signal generation element **30** depicted in **FIG. 3B** includes two antennae **36** and **37** attached to silicon chip **31**. Also shown are metals 1 and 2 (**32** and **33**). The assembly **30** includes circuitry on a silicon chip **31** with either two or four metal
10 structures (**32**, **33**, **36** and **37**) attached to it. In embodiments where two different metals are employed, the two metal structures serve as battery metals, that is metal 1 and metal 2 (**32** and **33**). These metal structures can be provided in a variety of forms. For instance, in one embodiment, metal 1 and metal 2 are very thick plated elements on the surface of the chip, front and back (e.g., as shown in
15 **FIG. 3C** described below). In another embodiment, metal 1 and metal 2 are relatively long wires that are simply bonded to the chip at some point, e.g., as shown in **FIG. 3B**. Metal 1 and metal 2 in some cases are insulated. In this case, the erosion occurs at the tip and then propagates towards the chip **31**. The erosion as it dissolves in the solution starts at the end of the wire and gradually
20 work its way toward the chip **31**. This configuration improves battery life. In another configuration, a metal is plated up on the front and back of the chip, and then the surface disappears. The two wires can also be employed as antennae. In one configuration, a perpendicular pair of antennae (**36** and **37**) are provided. In this implementation, there would be two other metal structures which are
25 typically of the same material. This material can be selected from a variety of metals, such as platinum or gold. These metal structures are attached to the chip and extend some dimension away from the chip. Typically these structures are on the order of a millimeter to a centimeter combined length. In some configurations, a significant portion of the metal structures are insulated so that
30 the dipole created is of maximum dimension. In other configurations, just the battery metals perform that dipole function, e.g., as described below in connection with **FIG. 3C**, or a separate antenna is provided.

In certain embodiments, the signal generation element does not include antennae and instead uses battery components as antennae, such as shown in

FIG. 3C. In **FIG. 3C**, signal generation element **30** includes silicon support layer **31** positioned between metal 1 layer **32** and metal 2 layer **33**. Also shown is circuitry layer **38**. In such embodiments, when a switch on the chip, e.g., in the circuitry layer, is closed, a current is produced between the two metals of the battery, which is then detected. In certain embodiments, a membrane larger than chip which defines a path for the current to travel is provided.

Yet another embodiment of a battery which is activated upon contact with a physiological fluid is shown in **FIGS. 3D** and **3E**. In the structure shown in these figures, the battery comprises top and bottom portions each supporting an electrode, where the top and bottom portions can be brought together to produce a structure comprising a volume bounded by opposing first and second electrodes, where the volume may be filled with an electrolyte, e.g., physiological fluid, when active. **FIG. 3D** provides a representation of a bottom portion **31A** of the battery in which material 1 **32A** is deposited into a recessed chamber **33A** on top of a substrate (e.g., silicon chip) **34A**. Recessed chamber **33A** has one or more ends open to allow electrolyte to enter. Material 2 **35A** is deposited on a separate substrate **36A** to produce a second portion **37A**, which is then bonded, e.g. by bonds **38A** and **38B**, to the chip in a "flip chip" type process. All processing can be done at the wafer scale. Where desired, the openings of the recessed chamber are filled with a degradable material, e.g., with a polymer, to control how quickly the battery is activated. Substrates **34A** and **36A** for materials **34A** and **35A** can be silicon, metal, or polymer/plastic. In certain embodiments, the structure shown in **FIGS. 3D** and **3E** is a battery where the first electrode is deposited into a recessed chamber on the top of the chip. The recessed space has one or two open ends to allow electrolyte flow. The second electrode is deposited on a separate substrate (e.g. a silicon wafer, a metal film or a polymer film), then bonded on top of the wafer with the chips on it in a "flip-chip" type process. The processing is done at a wafer scale and the cells diced as usual. The advantages of this configuration include: protection of the electrode surfaces from being blocked by components present in the stomach or the stomach lining itself; prevention of contact between any species generated on the battery (e.g., Cu) and the stomach lining that could have toxicity risks; 3) provision of uniform consumption of electrode materials across the electrode surface and more uniform current distribution between the electrodes.

FIG. 4 provides a diagrammatic representation of the events which occur when the pill is ingested and dissolved to the point that some of the pill has been chemically and/or physically eroded away. Metal 1 and metal 2 (**32** and **33**) are now in an ionic solution **39**. This creates a low voltage (V-) and a high voltage (V+) as applied to an electronic circuit **40**. The two outputs of that electronic circuit **40** are E0 **41** and E1 **42**, which are the signal-transmission electrodes on the top surface. In an alternate embodiment not shown in **FIG. 4** where the signal generation element **30** includes a single electrode, the output is E0 **41**.

FIG. 5 shows a similar arrangement as in **FIG. 4**. However, instead of having two electrodes as the output, a coil is provided. Metal 1 and metal 2 (**32** and **33**) are applied to the electronic circuit **40** of signal generation element **30**. The outputs of the electronic circuit **40** are coupled to a coil **43**. This configuration provides that a battery is created by metal 1 and metal 2 (**32** and **33**) when exposed to ionic solution. This battery drives the circuit **40**, which creates an oscillating frequency. This oscillating current goes through the coil and generates a RF magnetic signal. Unlike near-field quasi-static electrical signals, which may suffer from significant attenuation through body tissues, the RF magnetic signal can be transmitted through body tissues with less attenuation. The RF magnetic signal is then picked up by an external or internal receiver device that has a magnetic-signal detection mechanism. If a broadcast is provided at a high enough frequency, a pager-like device that is worn by the patient will detect whenever a pill is ingested.

FIG. 6B shows the detail of one implementation of an electronic circuit that can be employed in a signal generation element. On the left side are the two battery electrodes, metal 1 and metal 2 (**32** and **33**). These metals, when in contact with an electrolyte, form a battery and provide power to an oscillator **61**, in this case shown as a schematic. The metal 1 **32** provides a low voltage, (ground) to the oscillator **61**. Metal 2 **33** provides a high voltage (V_{high}) to the oscillator **61**. As the oscillator **61** becomes operative, it generates a clock signal **62** and an inverted clock signal **63**, which are opposites of each other. These two clock signals go into the counter **64** which simply counts the number of clock cycles and stores the count in a number of registers. In the example shown here, an 8 bit counter is employed. Thus, the output of counter **64** begins with a value of "00000000," changes to "00000001" at the first clock cycle, and continues up

to "11111111." The 8-bit output of counter **64** is coupled to the input of an address multiplexer (mux) **65**. In one embodiment, mux **65** contains an address interpreter, which can be hard-wired in the circuit, and generates a control voltage to control the oscillator **61**. Mux **65** uses the output of counter **64** to
5 reproduce the address in a serial bit stream, which is further fed to the signal-transmission driving circuit. Mux **65** can also be used to control the duty-cycle of the signal transmission. In one embodiment, mux **65** turns on signal transmission only one sixteenth of the time, using the clock counts generated by counter **64**. Such a low duty cycle conserves power and also allows other devices to transmit
10 without jamming their signals. The address of a given chip can be 8 bits, 16 bits or 32 bits. Typically, more than 8 bits will be used in a product because there are so many different types of pharmaceuticals. Each pharmaceutical will have its own specific address.

The present invention also allows the possibility that, where appropriate,
15 each pharmaceutical batch can be provided with a batch specific address. This allows identification of where the pill was made, when the pill was made, and in what batch it was made. In some cases, each pill will have a unique identifier. This would be particularly useful when drugs are more likely to be subsequently stolen or used illicitly, and thus should be tracked, or where questions of
20 contamination may arise.

According to one embodiment, mux **65** produces a control voltage, which encodes the address serially and is used to vary the output frequency of oscillator **61**. By example, when the control voltage is low, that is, when the serial address bit is at a 0, a 1 megahertz signal is generated by the oscillator. When the control
25 voltage is high, that is, when the address bit is a 1, a 2 megahertz signal is generated the oscillator. Alternately, this can be 10 megahertz and 20 megahertz, or a phase shift keying approach where the device is limited to modulating the phase. The purpose of mux **65** is to control the frequency of the oscillator or an AC alternative embodiment of the amplified signal of oscillation.

30 The outputs of mux **65** are coupled to electrode drive **66** which can drive the electrodes to impose a differential potential to the solution, drive an oscillating current through a coil to generate a magnetic signal, or drive a single electrode to push or pull charge to or from the solution.

In this manner, the device broadcasts the sequence of 0's and 1's which constitute the address stored in mux **65**. That address would be broadcast repeatedly, and would continue broadcasting until metal 1 or metal 2 (**32** and **33**) is consumed and dissolved in the solution, when the battery no longer operates.

5 **FIG. 7** is an alternate embodiment of the present invention. This implementation of the circuit **70** shows the oscillator **71** and a counter **72**. The mux **73** takes 5 bits from counter **72** as its input. On the upper right corner of **FIG. 7** is an exemplary circuit diagram for the signal-transmission electrode driver. Two CMOS invertors respectively take the clock and inverted clock signals
10 as their inputs, and drives electrodes e0 and e1.

FIG. 8 provides one implementation of an oscillator **80**. In this case, V_{control} **81** basically controls the amount of voltage driving the oscillator **80**. When V_{control} is low, a 20,000 ohm resistor **82** separates V_{low} **83**, which is the low power-supply voltage, and the oscillator control line, $V_{\text{osc_control}}$ **84**. When V_{control} is high, the
15 $V_{\text{osc_control}}$ goes to V_{low} , putting the maximum voltage across the oscillator circuitry and resulting in a higher frequency coming out of the clock signal and the inverted clock signal (**85** and **86**).

FIG. 9 shows a simple trickle or asynchronous counter which has in this case four flip flops with some simple inverters that simply count all the way up
20 and then start over again back to zero, and start counting all the way up again. In one embodiment, a multiplexer can take A0 and A1, A2, A3, as its address inputs and can compare these inputs with a stored address, and then have the stored address output as the oscillator control signal.

 As indicated above, in certain embodiments the signal generation element
25 may include a single electrode, and therefore have a monopole configuration. In one embodiment of the present invention, as shown in **FIG. 10**, a three terminal, monopole signal generation element **100** is provided. In this embodiment, the signal generation element **100** of the pill has one electrode **101** which is capacitively coupled to chip **107**. Two metal electrodes **103** and **102** constitute
30 the electrodes for the battery, which provides power for the signal generation element **100**. Electrodes **102** and **103** are coupled to the chip **107** through two resistors **104** and **105**, and an optional storage capacitor **106**. In one embodiment, electrode **102** is the ground and electrode **103** provides V_{high} for the signal generation element. Electrode **101** is the output of the mono pole signal

generation element. During operation, electrode 101 will push current into and out of body's fluid at a high frequency. A receiver will detect the pushing and pulling of that charge out of the body's fluids. Note that the biggest difference between this configuration and the configuration described previously is that this configuration provides a mono pole. When chip 107's output changes, capacitor 108 forces the potential on electrode 101 to change instantly, which result a corresponding change in the potential of the body. A receiver that is in contact of the body can thereby detect a large transient voltage change.

This inventive design produces an alternating current into and out of the body which is detected by a receiver (not shown). The output coupling capacitors may be optional. However, the presence of these capacitors prevents any DC currents and forces an AC signal.

FIG. 14 shows the multiplexer and the addressing system 73 of the circuitry of the signal generation element of **FIG. 7**. In this case, there are two 4 bit muxes (141 and 142) and a 1 bit mux 143, wherein the 1 bit mux 143 takes the outputs of the two 4 bit muxes 141 and 142 as its input. Each input port of muxes 141 and 142 is coupled to either the high voltage V_{high} or the low voltage V_{low} . This configuration of the present invention will allow for a 32 bit number, which is hard-wired to the 32 inputs of the two muxes, to be converted to a multiplexed serial output 144. As the counter goes through the 5 bits of counting, the output of mux 144 sequentially selects the inputs of muxes 141 and 142. When the 5 bit counter reaches "11111," the sequence will start over from the beginning again. This way the 16 bit address is repeatedly sent. An alternative approach is to send 16 bits of zeros and 16 bits of address alternatively, so that the receiving circuitry can be woken up and synchronized.

FIG. 15 shows a detail of the 4 bit mux 141 of the system shown in **FIG. 14**. The 4 bit mux is constructed from 4 levels of 1 bit muxes.

Fig. 16 shows the 1 bit mux in detail that makes up the 4 bit mux 141.

FIG. 17 is an additional mono pole embodiment 170 of a signal generation element. The biggest difference from the prior described embodiments is that a current source 171 is placed in series with the power supply created by M1 172 and M2 173. This creates a DC current between M1 172 and M2 173. This DC current does not compete with the AC signal generated by the electrode 174. This DC current will then go to one or another capacitor (175 and 176) and would

either charge up the electrode or charge up another capacitor. The concept behind this embodiment is to have a DC current created between M1 and M2 and an AC signal generated at the single electrode. Coupling capacitor 176 is optional.

5 **FIG. 18A** is an exemplary schematic diagram of a signal-transmission driver circuit. This circuit is based on an 8-pin 555 timer chip. As is shown on **FIG. 18A**, the pin designations of the 555 timer chip are as follows: pin 1 is the ground; pin 2 is the trigger, pin 3 is the output, pin 4 is reset, pin 5 is the control voltage, pin 6 is the threshold, pin 7 is discharge, and pin 8 is the power supply to
10 the chip V_{dd} . The output pin and the ground pin are capacitively coupled to two transmission electrodes, respectively. During operation, this circuit transmits a signal at a fixed frequency.

FIG. 18B1 to 18B2 is an exemplary schematic diagram of a receiver circuit. Shown on the upper left portion of the diagram is a front-end amplification
15 stage, which receives the signal through a pair of electrodes and performs differential amplification to the signal using an instrumentation amplifier. In the middle portion of the diagram is a cascaded four-stage filter. In one embodiment, the first two stages are high-pass filters with a cut-off frequency higher than 1 KHz, such as a cut-off frequency at approximately 10 KHz. The high-pass filter
20 removes the low-frequency noises and interferences, such as the 60 Hz power-line noise. The last two stages are low-pass filters with a cut-off frequency lower than 500 KHz, such as a cut-off frequency at approximately 200 KHz. The low-pass filters can remove high-frequency noises and interferences. The filtered and amplified signal is fed to an LED, as is shown on the lower left portion of the
25 diagram. When a signal is detected, the LED is lit indicating presence of the signal.

 The device described above generally includes two circuits: one is a logic circuit that generates the address bit sequence, and one is a driver circuit that drives the transmission electrodes based on the address bit sequence. The
30 power-consumption characteristics of these two circuits are different. Typically, the logic circuit requires a high voltage power supply, e.g., a 1.2 V power supply, to switch the CMOS circuits. However, the current drawn through the logic circuit

is relatively small. For example, in one embodiment, the current drawn through the logic circuits is approximately 5 μ A.

On the other hand, the driver circuit may draw a much larger current, because of the power it requires to transmit a sufficiently detectable signal. Consequently, the voltage of the power supply can be pulled down to a lower level. For example, the driver circuit can draw 100 μ A and pull the battery voltage down to 0.5 V.

Because the area of the battery electrodes can be limited due to the size constraint of the device, the interference between the two circuits with regard to power supply may be significant. As a result, the driver circuit could pull the battery voltage down to a point that makes the logic circuit inoperable. One embodiment of the present invention uses a split battery configuration to decouple the power supplies for the logic and driver circuits.

FIG. 19 shows one exemplary split (i.e., segmented) battery design. Two battery electrodes **193** and **194**, which are made from copper iodine, constitute the battery anodes for the logic circuit **191** and driver circuit **192**, respectively. Effectively, electrodes **193** and **194** form two separate batteries with a shared common magnesium cathode **195**. In this way, the driver circuit **192** can draw sufficient current to drive transmission electrodes **196** without significantly impairing the power supply for the logic circuit **191**.

During operation, driver circuit **192** draws a current from the battery formed by electrodes **194** and **195**, and pushes this current through transmission electrodes **196** into the body. In a further embodiment, the device can avoid the use of separate transmission electrodes by using the battery electrodes for transmission. **FIG. 20** shows such a configuration. The driver circuit **206** essentially contains a switch coupled between the anode **204** and the cathode. This switch can be turned on or off by the address signal from the logic circuit **201**. When the switch is turned on, the battery for the driver circuit is effectively short-circuited within the chip. Consequently, a current **207** flows through the body from the cathode to anode **204**. The resistance of the body tissue can thereby generate a voltage difference, which can be readily detected by, for example, a differential amplifier.

In some cases, the size of the cathode could be limited, resulting in coupling between the power supplies for the logic and driver circuits even with split anodes. According to one embodiment, as is shown in **FIG. 21**, the cathode can also be split to further decouple the two power supplies. Here, two separate
5 magnesium electrodes **211** and **212** serve as separate cathodes for the two batteries respectively serving the logic and driver circuits. The coupling between the two circuits can thus be minimized.

In a further embodiment, the battery electrodes for the driver circuit can be detached from the chip and coupled to the driver circuit through two external
10 wires, as is shown in **FIG. 22**. The battery electrodes for the logic circuit, on the other hand, can still be deposited on the chip to provide high-voltage power supply to the logic circuit. The external wires **221** and **222**, which can be approximately 1 cm long each, form a long dipole and can provide attendant signal amplification. As a result, the effectiveness of the transmission is not
15 limited by the size of the chip. In one embodiment, the wires are initially folded within a pill and can unfold when the pill is digested.

METHODS OF MAKING COMPOSITIONS

A variety of manufacturing protocols may be employed to produce
20 compositions according to the invention. In manufacturing the subject compositions, a signal generation element is stably associated with the pharmaceutical dosage form in some manner. By stably associated is meant that the signal generation element and the dosage form do not separate from each other, at least until administered to the subject in need thereof, e.g., by ingestion.
25 The signal generation element may be stably associated with the pharmaceutical carrier/active agent component of the composition in a number of different ways. In certain embodiments, where the carrier/active agent component is a solid structure, e.g., such as a tablet or pill, the carrier/active agent component is produced in a manner that provides a cavity for the signal generation element.
30 The signal generation element is then placed into the cavity and the cavity sealed, e.g., with a biocompatible material, to produce the final composition. For example, in certain embodiments a tablet is produced with a die that includes a feature which produces a cavity in the resultant compressed tablet. The signal generation element is placed into the cavity and the cavity sealed to produce the

final tablet. In a variation of this embodiment, the tablet is compressed with a removable element, e.g., in the shape of a rod or other convenient shape. The removable element is then removed to produce a cavity in the tablet. The signal generation element is placed into the cavity and the cavity sealed to produce the final tablet. In another variation of this embodiment, a tablet without any cavity is first produced and then a cavity is produced in the tablet, e.g., by laser drilling. The signal generation element is placed into the cavity and the cavity sealed to produce the final tablet. In yet other embodiments, a tablet is produced by combining the signal generation element with subparts of the tablet, where the subparts may be pre-made subparts or manufactured sequentially. For example, in certain embodiments tablets are produced by first making a bottom half of the tablet, placing the signal generation element on a location of the bottom half of the tablet, and then placing top portion of the tablet over the bottom half and signal generation element to produce the final desired composition. In certain embodiments, a tablet is produced around a signal generation element such that the signal generation element is located inside of the produced tablet. For example, a signal generation element, which may or may not be encapsulated in a biocompatible compliant material, e.g., gelatin (to protect the signal generation element), is combined with carrier/active agent precursor, e.g., powder, and compressed or molded into a tablet in a manner such that the signal generation element is located at an internal position of the tablet. Instead of molding or compressing, the carrier/active agent component is, in certain embodiments, sprayed onto the signal generation element in a manner that builds up the tablet structure. In yet another embodiment, the active agent/carrier component precursor may be a liquid formulation which is combined with the signal generation element and then solidified to produce the final composition. In yet other embodiments, pre-made tablets may be fitted with the signal generation element by stably attaching the signal generation element to the tablet. Of interest are protocols that do not alter the properties of the tablet, e.g., dissolution etc. For example, a gelatin element that snap fits onto one end of a tablet and has the chip integrated with it is employed in certain embodiments. The gelatin element is colored in certain embodiments to readily identify tablets that have been fitted with the signal generation element. Where the composition has an active agent/carrier composition filled capsule configuration, e.g., such as a

gelatin capsule filled configuration, the signal generation element may be integrated with a capsule component, e.g., top or bottom capsule, and the capsule filled with the active agent/carrier composition to produce the final composition. The above reviewed methods of manufacture are merely illustrative
5 of the variety of different ways in which the compositions of the invention may be manufactured.

SYSTEMS

Also provided are systems that include the subject compositions. Systems
10 of the subject invention include, in certain embodiments, one or more active agent containing compositions, e.g., as reviewed above, as well as a signal detection component, e.g., in the form of a receiver. The signal detection component may vary significantly depending on the nature of the signal that is generated by the signal generation element of the composition, e.g., as reviewed
15 above.

In certain embodiments, the signal detection component is an implantable component. By implantable component is meant that the signal detection component is designed, i.e., configured, for implantation into a subject, e.g., on a semi-permanent or permanent basis. In these embodiments, the signal detection
20 component is *in vivo* during use. In yet other embodiments, the signal detection component is *ex vivo*, by which is meant that the detection component is present outside of the body during use. In certain of these embodiments, as developed in greater detail below, either separate from or integrated with the *ex vivo* detection component may be a dosage dispenser element, e.g., for dispensing dosages of
25 the compositions based on signal detected from the signal generation element of the detector. Such features may also be present in implantable detection components, e.g., to provide a closed loop administration system that administers a subsequent dosage based on input about ingestion of a previous dosage.

As reviewed above, in certain embodiments the signal generation element
30 of the composition is activated upon contact with a target body site. In certain of these embodiments, the signal detection component is activated upon detection of a signal from the signal generation element. In certain of these embodiments, the composition generates an intermittent signal. In certain of these

embodiments, the detection element is capable of simultaneously detecting multiple compositions.

The signal detection component may include a variety of different types of signal receiver elements, where the nature of the receiver element necessarily varies depending on the nature of the signal produced by the signal generation element. In certain embodiments, the signal detection component may include one or more electrodes for detecting signal emitted by the signal generation element. In certain embodiments, the receiver device will be provided with two electrodes that are dispersed at some distance. This distance allows the electrodes to detect a differential voltage. In certain embodiments, the first electrode is in contact with an electrically conductive body element, e.g., blood, and the second electrode is in contact with an electrically insulative body element relative to said conductive body element, e.g., adipose tissue (fat). In an alternative embodiment, a receiver that utilizes a single electrode is employed. In certain embodiments, the signal detection component may include one or more coils for detecting signal emitted by the signal generation element. In certain embodiments, the signal detection component includes an acoustic detection element for detecting signal emitted by the signal generation element.

For those embodiments where the signal generated by the identifier is a near-field conductive signal, e.g., as reviewed above, the receiver of the present systems may also be viewed as "data collectors." As used herein, a "data collector" is any device equipped with receiving antenna to detect the potential differences created in the body by a transmitter as described above, thus receiving the information transmitted. A data collector may handle received data in various ways. In some embodiments, the collector simply retransmits the data to an external device (e.g., using conventional RF communication). In other embodiments, the data collector processes the received data to determine whether to take some action such as operating an effector that is under its control, activating a visible or audible alarm, transmitting a control signal to an effector located elsewhere in the body, or the like. In still other embodiments, the data collector stores the received data for subsequent retransmission to an external device or for use in processing of subsequent data (e.g., detecting a change in some parameter over time). It is to be understood that data collectors

may perform any combination of these and/or other operations using received data.

While the receiving antenna is advantageously inside the patient or in contact with the patient's skin, it is not required that data collector be entirely
5 internal to the patient. For instance, a watch or belt worn externally and equipped with suitable receiving electrodes can be used as a data collector in accordance with one embodiment of the present invention. The data collector may provide a further communication path via which collected data can be extracted by a patient or health care practitioner. For instance, an implanted collector may include
10 conventional RF circuitry (operating, e.g., in the 405-MHz medical device band) with which a practitioner can communicate, e.g., using a data retrieval device, such as a wand as is known in the art. Where the data collector includes an external component, that component may have output devices for providing, e.g., audio and/or visual feedback; examples include audible alarms, LEDs, display
15 screens, or the like. The external component may also include an interface port via which the component can be connected to a computer for reading out data stored therein.

In some embodiments, the data collector is implanted. For instance, as noted above, pacemaker leads provide a suitably sized receiving antenna.
20 Typical pacemakers include a control unit (referred to as a "can") that incorporates logic circuits configured to perform various data collection and processing operations. The can is also connected to RF transmitter/receiver circuitry that allows communication between the pacemaker and an external wand operated by a health care practitioner. Thus, where the patient has a
25 pacemaker, leveraging the existing unit as a data collector may be an efficient choice.

In certain embodiments, the system further includes an element for storing data, i.e., a data storage element. Typically, the data storage element is a computer readable medium. The term "computer readable medium" as used
30 herein refers to any storage or transmission medium that participates in providing instructions and/or data to a computer for execution and/or processing. Examples of storage media include floppy disks, magnetic tape, CD-ROM, a hard disk drive, a ROM or integrated circuit, a magneto-optical disk, or a computer readable card such as a PCMCIA card and the like, whether or not such devices are internal or

external to the computer. A file containing information may be "stored" on computer readable medium, where "storing" means recording information such that it is accessible and retrievable at a later date by a computer. With respect to computer readable media, "permanent memory" refers to memory that is permanent. Permanent memory is not erased by termination of the electrical supply to a computer or processor. Computer hard-drive ROM (i.e. ROM not used as virtual memory), CD-ROM, floppy disk and DVD are all examples of permanent memory. Random Access Memory (RAM) is an example of non-permanent memory. A file in permanent memory may be editable and re-writable.

10 In certain embodiments, the data that is recorded on the data storage element includes at least one of, if not all of, time, date, and an identifier of each composition administered to a patient, where the identifier may be the common name of the composition or a coded version thereof. In certain embodiments, the data of interest includes hemodynamic measurements. In certain embodiments, the data of interest includes cardiac tissue properties. In certain embodiments, the data of interest includes pressure or volume measurements.

15 The invention also provides computer executable instructions (i.e., programming) for performing the above methods. The computer executable instructions are present on a computer readable medium. Accordingly, the invention provides a computer readable medium containing programming for use in detecting and processing a signal generated by a composition of the invention, e.g., as reviewed above.

20 As such, in certain embodiments the systems include one or more of: a data storage element, a data processing element, a data display element, data transmission element, a notification mechanism, and a user interface. These additional elements may be incorporated into the receiver and/or present on an external device, e.g., a device configured for processing data and making decisions, forwarding data to a remote location which provides such activities, etc.

30 In certain embodiments, the signal detection component includes a cardiac monitoring element, such as shown in the system of FIG. 1. FIG.1 shows a human 10 who has an implanted cardiovascular device "can" 8 and a lead 6, which components are employed to monitor and detect the signal emitted from pill 14. The monitoring device can be positioned in other locations as well, such

as subcutaneously, in the heart, or in the waist near the stomach, for example. Positioning may be suggested by a particular application.

The inventive monitoring system can also be positioned as an external device. By example, it could be positioned by a harness that is worn outside the
5 body and has one or more electrodes that attach to the skin at different locations. The inventive construct can be linked to a portable device, for example a watch that has one or two electrodes dispersed on the wrist. There are many places where such a receiving electrode system could be placed and created such as, hearing aids that beep, necklace, belt, shoes (PZT – powered), or earrings.

10 As indicated above, in certain embodiments the systems include an external device which is distinct from the receiver (which may be implanted or topically applied in certain embodiments), where this external device provides a number of functionalities. Such an apparatus can include the capacity to provide feedback and appropriate clinical regulation to the patient. Such a device can
15 take any of a number of forms. By example, the device can be configured to sit on the bed next to the patient. The device can read out the information described in more detail in other sections of the subject patent application, both from pharmaceutical ingestion reporting and from psychological sensing devices, such as is produced internally by a pacemaker device or a dedicated implant for
20 detection of the pill. The purpose of the external apparatus is to get the data out of the patient and into an external device. One feature of external apparatus is its ability to provide pharmacologic and physiologic information in a form that can be transmitted through a transmission medium, such as a telephone line, to a remote location such as a clinician or to a central monitoring agency.

25 In certain embodiments, the cardiac monitoring element includes a conduction velocity measurement element. In certain embodiments, the cardiac monitoring element includes a pressure sensor. In certain embodiments, the cardiac monitoring element includes a dimension sensor.

30 Additional physiological sensors with various designs have been described in additional applications by some of the present inventors. These sensors can be used jointly with the present inventive systems. In addition, other applications by some of the present inventors describe multiplexing systems with which the present invention can be very usefully employed in an interactive, synergistic manner.

This prior work by some of the present inventors describes the use of dimension sensors to determine heart parameters in order to facilitate appropriate therapy intervention, such as resynchronization therapy. Using the present invention to determining the time of blood-stream absorption of cardiac treatment pharmaceutical and correlating this with changes produced in heart function sensed by those devices provides highly valuable information for the clinician in titrating medications and providing synergy between pharmacological and electrophysiological treatment.

Embodiments of the present invention can be used in various systems. Such systems may include various types of sensors. Such sensors and systems have been described in various applications by some of the present inventors. These applications also describe multiplexing systems previously developed by some of the present inventors with which the present invention can be employed. These applications include: U.S. Patent Application No. 10/734490 published as 20040193021 titled: "Method And System For Monitoring And Treating Hemodynamic Parameters"; U.S. Patent Application No. 11/219,305 published as 20060058588 titled: "Methods And Apparatus For Tissue Activation And Monitoring"; International Application No. PCT/US2005/046815 titled: "Implantable Addressable Segmented Electrodes"; U.S. Patent Application No. 11/324,196 titled "Implantable Accelerometer-Based Cardiac Wall Position Detector"; U.S. Patent Application No. 10/764,429, entitled "Method and Apparatus for Enhancing Cardiac Pacing," U.S. Patent Application No. 10/764,127, entitled "Methods and Systems for Measuring Cardiac Parameters," U.S. Patent Application No. 10/764,125, entitled "Method and System for Remote Hemodynamic Monitoring"; International Application No. PCT/ US2005/046815 titled: "Implantable Hermetically Sealed Structures"; U.S. Application No. 11/368,259 titled: " Fiberoptic Tissue Motion Sensor"; International Application No. PCT/US2004/041430 titled: "Implantable Pressure Sensors,"; U.S. Patent Application No. 11/249,152 entitled "Implantable Doppler Tomography System," International Application Serial No. PCT/USUS05/39535 titled "Cardiac Motion Characterization by Strain Gauge".

Some of the present inventors have developed a variety of display and software tools to coordinate multiple sources of sensor information. Examples of these can be seen in PCT application serial no. PCT/US2006/12246 titled: "Automated Optimization of Multi-Electrode Pacing for Cardiac Resynchronization" and filed on March 31, 2006.

The above described systems are reviewed in terms of communication between an identifier on a pharmaceutical composition and a receiver. However, the systems are not so limited. In a broader sense, the systems are composed of two or more different modules that communicate with each other, e.g., using the transmitter/receiver functionalities as reviewed above, e.g., using the monopole transmitter (e.g., antenna) structures as described above. As such, the above identifier elements may be incorporated into any of a plurality of different devices, e.g., to provide a communications system between two self-powered devices in the body, where the self-powered devices may be sensors, data receivers and storage elements, effectors, etc. In an exemplary system, one of these devices may be a sensor and the other may be a communication hub for communication to the outside world. This inventive embodiment may take a number of forms. There can be many sensors, many senders and one receiver. They can be transceivers so both of these can take turns sending and receiving according to known communication protocols. In certain embodiments, the means of communication between the two or more individual devices is the mono polar system, e.g., as described above. In these embodiments, each of these senders may be configured to take turns sending a high frequency signal into the body using a monopole pulling charge into and out of the body which is a large capacitor and a conductor. The receiver, a monopole receiver is detecting at that frequency the charge going into and out of the body and decoding an encrypted signal such as an amplitude modulated signal or frequency modulated signal. This embodiment of the present invention has broad uses. For example, multiple sensors can be placed and implanted on various parts of the body that measure position or acceleration. Without having wires connecting to a central hub, they can communicate that information through a communication medium.

METHODS

In the methods of the subject invention, an effective amount of a composition of the invention is administered to a subject in need of the active agent present in the composition, where "effective amount" means a dosage sufficient to produce the desired result, e.g. an improvement in a disease condition or the symptoms associated therewith, the accomplishment of a desired physiological change, etc. The amount that is administered may also be viewed as a therapeutically effective amount. A "therapeutically effective amount" means the amount that, when administered to an subject for treating a disease, is sufficient to effect treatment for that disease.

The composition may be administered to the subject using any convenient means capable of producing the desired result, where the administration route depends, at least in part, on the particular format of the composition, e.g., as reviewed above. As reviewed above, the compositions can be formatted into a variety of formulations for therapeutic administration, including but not limited to solid, semi-solid or liquid, such as tablets, capsules, powders, granules, ointments, solutions, suppositories and injections. As such, administration of the compositions can be achieved in various ways, including, but not limited to: oral, buccal, rectal, parenteral, intraperitoneal, intradermal, transdermal, intracheal, etc., administration. In pharmaceutical dosage forms, a given composition may be administered alone or in combination with other pharmaceutically active compounds, e.g., which may also be compositions having signal generation elements stably associated therewith.

The subject methods find use in the treatment of a variety of different conditions, including disease conditions. The specific disease conditions treatable by with the subject compositions are as varied as the types of active agents that can be present in the subject compositions. Thus, disease conditions include, but are not limited to: cardiovascular diseases, cellular proliferative diseases, such as neoplastic diseases, autoimmune diseases, hormonal abnormality diseases, infectious diseases, pain management, and the like.

By treatment is meant at least an amelioration of the symptoms associated with the disease condition afflicting the subject, where amelioration is used in a broad sense to refer to at least a reduction in the magnitude of a parameter, e.g.

symptom, associated with the pathological condition being treated. As such, treatment also includes situations where the pathological condition, or at least symptoms associated therewith, are completely inhibited, e.g. prevented from happening, or stopped, e.g. terminated, such that the subject no longer suffers
5 from the pathological condition, or at least the symptoms that characterize the pathological condition. Accordingly, "treating" or "treatment" of a disease includes preventing the disease from occurring in an animal that may be predisposed to the disease but does not yet experience or exhibit symptoms of the disease (prophylactic treatment), inhibiting the disease (slowing or arresting its
10 development), providing relief from the symptoms or side-effects of the disease (including palliative treatment), and relieving the disease (causing regression of the disease). For the purposes of this invention, a "disease" includes pain.

A variety of subjects are treatable according to the present methods. Generally such subjects are "mammals" or "mammalian," where these terms are
15 used broadly to describe organisms which are within the class mammalia, including the orders carnivore (e.g., dogs and cats), rodentia (e.g., mice, guinea pigs, and rats), and primates (e.g., humans, chimpanzees, and monkeys). In representative embodiments, the subjects will be humans.

In certain embodiments, the subject methods, as described above, are
20 methods of managing a disease condition, e.g., over an extended period of time, such as 1 week or longer, 1 month or longer, 6 months or longer, 1 year or longer, 2 years or longer, 5 years or longer, etc. The subject methods may be employed in conjunction with one or more additional disease management protocols, e.g., electrostimulation based protocols in cardiovascular disease
25 management, such as pacing protocols, cardiac resynchronization protocols, etc; lifestyle, such a diet and/or exercise regimens for a variety of different disease conditions; etc.

In certain embodiments, the methods include modulating a therapeutic regimen based data obtained from the compositions. For example, data may be
30 obtained which includes information about patient compliance with a prescribed therapeutic regimen. This data, with or without additional physiological data, e.g., obtained using one or more sensors, such as the sensor devices described above, may be employed, e.g., with appropriate decision tools as desired, to make determinations of whether a given treatment regimen should be maintained

or modified in some way, e.g., by modification of a medication regimen and/or implant activity regimen. As such, methods of invention include methods in which a therapeutic regimen is modified based on signals obtained from the composition(s).

5 In certain embodiments, also provided are methods of determining the history of a composition of the invention, where the composition includes an active agent, an identifier element and a pharmaceutically acceptable carrier. In certain embodiments where the identifier emits a signal in response to an
10 interrogation, the identifier is interrogated, e.g., by a wand or other suitable interrogation device, to obtain a signal. The obtained signal is then employed to determine historical information about the composition, e.g., source, chain of custody, etc.

 In yet other embodiments where the identifier is one that survives digestion, the methods generally include obtaining the signal generation element
15 of the composition, e.g., by retrieving it from a subject that has ingested the composition, and then determining the history of the composition from obtained signal generation element. For example, where the signal generation element includes an engraved identifier, e.g., barcode or other type of identifier, the engraved identifier may be retrieved from a subject that has ingested the
20 composition and then read to identify at least some aspect of the history of the composition, such as last known purchaser, additional purchasers in the chain of custody of the composition, manufacturer, handling history, etc. In certain embodiments, this determining step may include accessing a database or analogous compilation of stored history for the composition.

25

UTILITY

 The present invention provides the clinician an important new tool in their therapeutic armamentarium: automatic detection and identification of pharmaceutical agents actually delivered into the body. The applications of this
30 new information device and system are multi-fold. Applications include, but are not limited to: (1) monitoring patient compliance with prescribed therapeutic regimens; (2) tailoring therapeutic regimens based on patient compliance; (3) monitoring patient compliance in clinical trials; (4) monitoring usage of controlled

substances; and the like. Each of these different illustrative applications is now reviewed in greater detail below.

Monitoring Patient Compliance with Prescribed Therapeutic Regimens

5 As summarized above, one type of application in which the subject compositions and systems find use is in monitoring patient compliance with prescribed therapeutic regimens. By monitoring patient compliance is meant tracking whether a patient is actually taking medication in the manner prescribed to the patient. As such, the present invention provides accurate data of when a
10 pill has been taken and which pill has been taken. This allows the precise determination of which pill was taken at a specific point in time. Such monitoring capability assures patients are taking the prescribed medication correctly. This information avoids the potential for over prescription of medications that are not actually being taken. By example, if pain killers are intended to be administered
15 to a patient, it is possible to verify with the present invention that the patient did in fact take those pain killers in a certain period of time. This knowledge is an important tool in limiting the illicit sale of unconsumed drugs to an unintended party. In the case of cardio vascular pills, the clinician or care giver is able to verify that the amount of the drug was taken has been taken at approximately the
20 right point and time. Thus, the true efficacy of the drug can be accurately evaluated. Proper administration and patient compliance is especially critical in Alzheimer's, psychiatric, and alcohol aversion drugs, and in the treatment of rest home residents. In the case of accidental and other overdoses situations, the intervening clinician will be able to discern how far the ingestion has proceeded,
25 and how many pills are involved.

 In more complex embodiments of the present invention, correct, timely ingestion of the drugs will automatically trigger a prescription refill signal which is forwarded to a pharmacy data system, and in some cases the refill will be automatically delivered directly to the patient's home, or released by a device in
30 the patient's home some period of time later. This feature is particularly valuable in patients with compromised mental capacity and/or limited physical mobility.

 The invention is particularly useful in complex administration regimens, such as when multiple pharmaceuticals are being taken, and confusion is more likely to occur. The inventive pills can have multiple external layers, with only

correct dosage allowing dissolution and absorption of the pharmaceutical component. Specific indicators, such as electrical conduction velocity in the heart or electrolytic levels in the blood in response to pharmaceutical can also be titrated.

5 In certain embodiments, a patient can be alerted when the patient is in some way non-compliant with a given treatment regimen. For example, by a sound, visual, or computer reminder, if the pharmacological regimen is not being accurately adhered to, a reminder is provided. If that reminder is not accurately responded to, the system can provide an alert to family members, caregivers, or
10 clinicians in order to remedy the gap in treatment or overdose. The device may also automatically modify the dosage and timing of the regimen to compensate for prior non-standard dosing.

Tailoring Therapeutic Regimens Based on Patient Compliance

15 As summarized above, one type of application in which the subject compositions and systems find use is in tailoring therapeutic regimens based on patient compliance. In such applications, data obtained about whether a patient has or has not taken a particular dosage is employed to determine future dosages and/or timing of such dosages. In certain embodiments, data concerning
20 patient compliance is combined with additional data, e.g., sensed physiological data, to make customized changes or modifications to a given therapeutic regimen. By example, when data about dosage compliance obtained according to the invention is used in concert with other medical sensing devices, correlation between drug delivery, batch and dosage can be correlated to a physiological
25 response. In this manner, optimal pharma-therapeutic regimens may be formulated by the clinician. By example, cardiac stimulating drugs can be titrated to the most appropriate dosages, minimizing side effects such as cardiac muscle exhaustion and rebound effects among others, and optimizing both dosage and timing for each individual patient.

30 Assessment of a range of alternate medications is made possible by the present invention without resort to awaiting overt clinical sequel of treatment, many of which can be seriously adverse. By example, positive effects would be quickly ascertainable without being obscured by more random factors. Negative

responses, such as changes in blood pressure, would become clearly evident as drug related or independent above background physiologic variation.

In one clinical arena, the present invention allows, in concert with other sensing devices developed by some of the present inventors, the measurement
5 and assessment of the cardiac response to those medications. These co-employed sensing devices can be those enumerated below, among others. Other sensing technology, e.g., as mentioned above, developed by some of the present inventors allows measurement of heart health and cardiac efficiency. Using these tools in concert with the present inventive device, the clinician will be
10 able to compare the response of the heart and body to the administered pharmaceutical. The data provided by the present invention can optionally be recorded over time. The recording system records synchrony or conduction velocity of a signal going through cardiac tissue and how that is mediated by the presence of a certain medication. This unique data is made possible by the
15 present invention since it can determine electronically exactly when the pill or other medication was being absorbed into the body.

In more standard clinical environments, this unique data allows careful selection and titration of drug administration without resort to more overt physical symptoms to ascertain contraindications, efficacy, and optimal dosage levels.
20 The present invention provides a record for emergency room technicians or doctors when a patient is admitted to a hospital so that the patient's status can be accurately ascertained. Dosage events within the last hour or day prior to admission, and the identity of the last medication, will be immediately available. As such, future therapeutic regimens can be made based on accurate records of
25 patient drug medication history.

In certain embodiments, the clinician obtains this information through simple interrogation of the implanted or portable device. This device would tell them without any uncertainty what pills have been taken. As the inventive technology becomes more wide spread, this data will become more regularly
30 available. The present inventive microchips are sufficiently inexpensive such that when they are put into standard production, most or all pharmaceuticals will be fitted with them as a matter of course.

The patient monitoring capacity of the external reporting apparatus is an importation function which the inventive device can provide. When coordinated

with internal or external physiologic sensing data, the device can read out the physiological response of the patient to the ingestion of medication, and then transmit this information back to the clinician. The clinician can then modify therapy to optimal effectiveness, as indicated by the new data in response to the modified therapy, and so forth.

In more sophisticated embodiments of the present invention, the dosage adjustment function, within certain parameters, can be performed by an intelligence circuit in the apparatus. By example, for a blood pressure medication, the patient takes their blood pressure pill. 20 minutes later, the internal monitoring circuitry in the implantable device registers a drop in blood pressure. The circuitry quantifies this drop, and transmits it to this bedside apparatus. The apparatus then can adjust the dosage of the pill to optimally treat the patient. Similarly, when the patient is connected to an IV, the dosage can be dispensed directly into the IV fluid. In certain embodiments, the closed-loop system is provided as a fully implantable device.

Current clinical practice for drug treatment optimization is considerably more limited than that which is available by use of the present inventive device. Currently, blood pressure medication treatment is set at so many pills per day. Such a blunt dosage regime takes a long time to optimize appropriately because the feedback loop is very slow. By contrast, with the present invention, the feedback loop of physiologic response to pharmaceutical dosage is very rapid and very efficient. Ultimately, the present invention allows tailoring the drug dosages day to day, or even more finely, to account for change in activity, change in physiological conditions in the patient, and other dosage parameter.

In more sophisticated embodiments of the present invention, physiological reactions to specific dosages and time intervals would also be continually monitored. In some embodiments, the level of drug in the blood stream is monitored, allowing for individual and time of day variations in drug metabolism.

This aspect of the present invention effectively minimizes underdosing or overdosing the controlled substances, in some cases addressing these changes before they produce external symptoms apparent to the patient or clinician. The drug dosage can be automatically titrated so that, by example, the smallest appropriate level to quell anxiety due to pain, other physiologic reactions to pain, or provide steady or gradually diminishing blood levels of the drug would be

dispensed. This feature of the present invention provides an automatic, appropriately gradual, weaning off of the drug, lessening the chance of serious addiction or severe, adverse withdrawal reactions.

5 Clinical Trial Applications

An important application of the invention is to provide immediate feedback of physiological data response to administration of a pharmaceutical agent in clinical drug trails. A current challenge is that the experimental drug is administered broadly to a population without a comprehensive foreknowledge of
10 which sub-groups within this population are most likely to benefit from the treatment. Another challenge is monitoring patient compliance with the treatment regimen, by determining if the tests subjects are taking the medicine as indicated. The later challenge is addressed in the sections above. Both patient non-compliance levels and actual response to drug ingestion can thus be determined.
15 As such, compliance intervention can then be addressed early in the study.

In certain embodiments of the present invention, clinical researchers are provided with immediate access to physiological data. The clinical researchers are able to identify the subset for whom the drug is most likely effective from within the original test population of possible participants in the trial. The example
20 above of a patient receiving blood pressure medication and getting feedback immediately demonstrates how effectiveness of a novel medicine can be quickly determined.

Upon administration of the first doses of medication to initial test subjects, the clinical researchers are likely to find that some subjects in the population
25 respond to the medication and others do not. This immediate feedback allows the administrator of the trail to exclude those patients who do not respond to the medication and target only that subgroup for whom there is clear efficacy. This culling process allows the overall results of the trail to get a much higher effective percentage, because one is able to target the drug to the group for whom it is
30 effective. It also avoids side effect challenges for subjects who would not have a benefit balance to such risks.

As such, from this innovative data, the present invention provides the clinician an accurate dose response curve showing the response to that medication and the timing of the digestion of the pill. Such innovative data has

many applications. For instance, the clinician now has the ability to determine which patients have no response to the medicine in the pill. In a study situation, such patients can be removed from a study or a test of the clinical utility of a certain medication. This ability provides that only people who have a beneficial
5 response to a certain medication are retained in the trail. This feature will improve the efficacy of medications and to reduce the amount of medications that people take that are not being useful. It may also be used in trials to determine which patients actually consumed the medicine, and which did not.

The present invention allows identification of physiological proxies for the
10 efficacy of a drug. By example, for a drug which has a long term administration prior to the development of overt clinical changes, there are typically certain short term physiological factors which appear immediately after ingestion of the drug. By example, cancer medication which requires many months to show an effect, can have shorter term indicia of its efficacy in one or a constellation of physiologic
15 factors. Changes, both local or throughout the whole body, in blood pressure, body temperature, internal chemical enzymes or other factors will serve as proxies for the longer term desired effects. A precise correlation of these factors with the time of the pills ingestion enhances the ability to find meaningful indicia.

With the very closely timed correlated response to the ingestion of the pill
20 provided for the first time by the present innovation, demonstrating that a physiologic response is a result of the drug ingestion rather than any of the other possibility confounding factors, is much more likely. This capacity of the present invention can serve as a partial or complete proxy for clinical trials.

The invention provides a way to determine very quickly whether a patient
25 should be taking the medication or not, whether it will be effective or not, and allow its appropriate titration. Synergies between medications, both helpful and adverse, will also become more readily apparent.

Monitoring Usage of Controlled Substances

30 As reviewed above, in other embodiments of the inventive microchips, the identifiers can be fitted with coils, susceptible of interrogation without being dissolved in the body. This is accomplished by transmitting RF energy into the coil in such a way that the inquirer will be apprised of the presence and identity of a pill before it is ingested.

In an additional embodiment of the present invention, a "smart box" is provided that can interrogate each pill and ascertain its address. The box can write a distinctive product number or product code so that every single pill ever made is provided with a unique identifier. Fuses, for example, may be selectively
5 destroyed so the addresses may be detected electrically or optically. Particularly in the case of controlled substances, such as a narcotic, this will be important in limiting the illegal use of previously legitimate medicines. The present invention makes it possible to identify precisely who bought such a pill from the authorized pharmacist. This use of the present invention will rein in the number of illicit uses
10 of controlled substances on the market place.

An important application for the external apparatus aspect of the present invention is in monitoring and regulating the use of controlled pharmaceutical substances. A serious risk when patients are prescribed heavy narcotics for pain control is the possibility of addiction. In its simplest analysis, addiction occurs
15 from the ingestion of too much of the controlled medication by inadvertent overdosing, purposeful misuse, or through inexact dosage prescription. Additionally, as described above, individual serial numbers are provided on such pharmaceuticals to track the legitimate distribution of the drug before the illicit distribution of such drugs.

20 In one application of the present invention, a means for locking and regulating the dosage of a potential addictive drug is provided. An example of this capacity of the present invention is when a patient takes their narcotic pill, in which the ingestion of the medication is registered by the internal device. This information is then automatically transmitted to the external apparatus.

25 The inventive apparatus is so configured that only after the patient has taken the pill and at the appropriate time has elapsed does this accessory apparatus dispense a further pill. In this manner, the addiction rate for the drug is dramatically lowered by limiting legal drug availability by dispensing exactly the prescribed dosage at precisely the appropriate time interval.

30 The external apparatus can also be effectively employed in mandatory medication forensic applications. For example, in the case of a convicted criminal, the criminal can be required to take court ordered medication as a condition of release from jail. Using the present invention, the court or probation officer has access to a real-time record of the administration of this drug as this

information is fed back through the accessory apparatus to the appropriate official. There is a current trend towards court mandated psychotropic or chemical sterilization drug maintenance for sex offenders which would be addressed by this aspect of the present invention. This use of the present
5 invention is analogous to house arrests where physical position monitoring bands are worn on the ankle of the offender.

KITS

Also provided are kits for practicing the subject methods. Kits may include
10 one or more compositions of the invention, as described above. The dosage amount of the one or more pharmacological agents provided in a kit may be sufficient for a single application or for multiple applications. Accordingly, in certain embodiments of the subject kits a single dosage amount of a pharmacological agent is present and in certain other embodiments multiple
15 dosage amounts of a pharmacological agent may be present in a kit. In those embodiments having multiple dosage amounts of pharmacological agent, such may be packaged in a single container, e.g., a single tube, bottle, vial, and the like, or one or more dosage amounts may be individually packaged such that certain kits may have more than one container of a pharmacological agent.

20 Suitable means for delivering one or more pharmacological agents to a subject may also be provided in a subject kit. The particular delivery means provided in a kit is dictated by the particular pharmacological agent employed, as describe above, e.g., the particular form of the agent such as whether the pharmacological agent is formulated into preparations in solid, semi solid, liquid
25 or gaseous forms, such as tablets, capsules, powders, granules, ointments, solutions, suppositories, injections, inhalants and aerosols, and the like, and the particular mode of administration of the agent, e.g., whether oral, buccal, rectal, parenteral, intraperitoneal, intradermal, transdermal, intracheal, etc. Accordingly, certain systems may include a suppository applicator, syringe, I.V. bag and
30 tubing, electrode, etc.

In certain embodiments the kits may also include a signal receiving element, as reviewed above. In certain embodiments, the kits may also include an external monitor device, e.g., as described above, which may provide for

communication with a remote location, e.g., a doctor's office, a central facility etc., which obtains and processes data obtained about the usage of the composition.

The subject kits may also include instructions for how to practice the subject methods using the components of the kit. The instructions may be recorded on a suitable recording medium or substrate. For example, the instructions may be printed on a substrate, such as paper or plastic, etc. As such, the instructions may be present in the kits as a package insert, in the labeling of the container of the kit or components thereof (i.e., associated with the packaging or sub-packaging) etc. In other embodiments, the instructions are present as an electronic storage data file present on a suitable computer readable storage medium, e.g. CD-ROM, diskette, etc. In yet other embodiments, the actual instructions are not present in the kit, but means for obtaining the instructions from a remote source, e.g. via the internet, are provided. An example of this embodiment is a kit that includes a web address where the instructions can be viewed and/or from which the instructions can be downloaded. As with the instructions, this means for obtaining the instructions is recorded on a suitable substrate.

Some or all components of the subject kits may be packaged in suitable packaging to maintain sterility. In many embodiments of the subject kits, the components of the kit are packaged in a kit containment element to make a single, easily handled unit, where the kit containment element, e.g., box or analogous structure, may or may not be an airtight container, e.g., to further preserve the sterility of some or all of the components of the kit.

The following example is offered by way of illustration and not by way of limitation.

EXPERIMENTAL

Example 1.

In the following experiment, a transmitter (Tx) and receiver (Rx), each powered by batteries and encased in a water-tight Rubbermaid™ container, are employed. The Tx and Rx float in a bath of saline, and an LED glows on the Rx

when the Tx is placed in the bath. Both Tx and Rx are completely isolated from the outside world.

The Tx, representing the compositions of the present application, e.g., a pill composition having an active agent and signal generation element, is an oscillator circuit based on a CMOS timer chip. It produces a square wave at about 80 kHz of 3V amplitude from a Lithium battery. A tightly twisted pair of wires extends from the circuit, out of the container, and into the bath. At the end of the twisted pair, the wires are striped of insulation by about 1mm and separated to form a dipole antenna. The signal amplitude was found to scale linearly with the separation distance characterizing this dipole. The signal was easily detectable with this setup when the dipole was 5mm in extent.

The Rx is a filtered amplifier circuit with outputs to detect the transmitted signal. A square of copper, 10cm on a side, was attached to the bottom of the outside of the container and attached to the negative differential input of the circuit; this represents the pacing can. A bipolar pacing lead, about 40cm long, was attached to the positive differential input of the circuit; the ring electrode was selected for the input. The differential signal was coupled into the inputs of a gain 100 instrumentation amplifier through 0.1uF series capacitors. The output of the instrumentation amplifier was fed into a 4-pole high-pass filter, with gain of 100 and cutoff frequency 5 kHz. This output was fed into a 2-pole low-pass filter with gain 20 and cutoff frequency 100 kHz. Thus, the overall gain of the circuit is 200,000. This output signal is applied across an LED and resistor in series, which glows when the output signal exceeds a few volts.

When not in the bath, the Rx LED was on all the time as it picked up interference and power line noise from the environment. When the pacing lead was shorted to the mock can the LED turned off.

When placed in solution, the LED turned off. When the Tx was also placed in solution, the Rx LED turned on and the dependence on position and orientation was investigated. The intensity of the LED was found to depend on the cosine of the angle between the Rx and Tx dipole, with a null for perpendicular orientation and sign inversion as the sense of the dipole was reversed, as observed with an external oscilloscope. The intensity of the LED was found to vary directly with position, with a bright, saturated glow observed for spacing less than 5cm and a dim, diffuse glow observed for the maximum

spacing allowed by the bath, about 50cm.

The key to making the detection robust is differentiating the desired signal from spurious interference. Such was accomplished in this experiment by restricting the frequency band of sensitivity to between 5 and 100 kHz. To the extent this band can be narrowed, the more robust the system will be. The challenge here is to match the frequency of the Tx and Rx circuits, in light of the fact that the Tx frequency may vary by 30% due to manufacturing variation. The Rx circuit can be very narrow through the use of a narrow bandpass or by using demodulation techniques from the radio. The Rx circuit can be swept across a tuning frequency range to detect the presence of the pill. The presence of the pill can be confirmed by encoding an unlikely bit sequence in the digital information transmitted by the pill.

Two problems with this approach are that it consumes power from the Rx circuit while it scans frequencies, and that synchronization with multiple pills, which may burst the transmission of their codes, is difficult. If the frequency of the Tx is known ab initio, as is possible with circuit trimming or advanced manufacturing processes, an elegant solution to both these problems is presented. At the input to the Rx circuit, a tuned LC oscillator matched to the Tx frequency will "ring up" when the desired signal is present. This power can be detected by a simple diode circuit, which serves as a trigger to turn the detection circuit on, greatly reducing the time it must draw current. This tuned input also serves to narrow the bandwidth and reject spurious signals.

This above experiment demonstrates the ability to transmit and detect signals through a synthetic biological medium. The Tx may be readily powered off a chemical battery, such as a Pt/Mg system. Furthermore, digital information is readily encoded in the signal using a variety of encoding techniques to eliminate errors and improve the overall reliability of the system.

Example 2.

A transmitter according to the subject invention was set up as follows. The circuit was powered off a 9V battery and floated on a bath of saline. The circuit was an oscillator based on the TLC551 chip, a CMOS version of the popular 555 timer. The oscillator was run at ~7 kHz, with a duty cycle of perhaps 15%. The outputs of the oscillator were each capacitively coupled through 7 uF to a twisted

pair, which was terminated in a small "Y" shaped dipole, with the arms separated by ~1mm, and ~2mm of bare wire exposed to the saline bath.

The signal was received through two Cu electrodes, each with ~1 cm² exposed to the bath. This was routed to the input of a Stanford pre-amp operated off batteries, set to a gain of 1000 with a pass band between 3 kHz and 30 kHz. The output of the pre-amp was observed on a battery powered oscilloscope.

A maximum signal of ~200 uV referenced to the amplifier input was observed for an Rx electrode separation of ~20 cm. A dipolar coupling strength was observed, displaying a sinusoidal angular dependence, with a null in received signal for perpendicular orientation; phase inversion was seen between parallel and anti-parallel orientations. The received signal strength was seen to scale linearly with separation of the Rx electrodes.

The above demonstrates that the signal is clearly detectable with proper amplification and filtering. Furthermore, a capacitor on the input of the Rx amplifier is not necessary; as the same results were obtained using DC coupling on the input with a high-pass filter later in the signal chain.

The above results also verified that the Tx can run off an Mg/Pt potato battery.

Example 3.

A prototype smart pill microchip, which broadcasts a fixed code using frequency shift keying, was first powered by a 1.5V AA battery. The conductive signal was applied to a physiological saline bath with a twisted pair T-shaped dipole, approximately 1 cm across with 1 mm of conductor exposed on each arm of the T. The signal was detected by two copper electrodes, spaced approximately 10 cm apart, which feed into a battery powered, isolated differential pre-amp. The signal was observed on an oscilloscope. An oscillatory signal, clearly representative of the transmitted data, was observed with a frequency of about 300 kHz and an input-referenced amplitude of about 10 mV. Furthermore, a dependence of the received signal strength on the cosine of the angle between the transmit and receive conductors, as is characteristic of a dipolar interaction, was observed.

A Mg-CuI water-activated battery, with each electrode having an exposed surface area of ~1 mm² was constructed. The Mg electrode was formed by

simply potting commercial grade Mg ribbon in epoxy and polishing the end flat with sandpaper. The CuI electrode was produced by first polishing the end of Cu wire potted in epoxy.

Approximately 100 μm of Cu was then electroplated on the end of the Cu wire using standard techniques, with the parameters chosen to give a large roughness coefficient, increasing the effective area of the electrode. The surface of this plated Cu was then transformed electrochemically to CuI by applying a potential corresponding to the potential of the Cu^+ ion in a solution of I^- ions. In approximately 15 min 40 mC of CuI was produced. The battery was demonstrated to have an open cell voltage of $\sim 1.05\text{V}$ in a pH 2 solution, corresponding to the acidity of a typical stomach.

The CuI-Mg battery was connected to the power terminals of the chip, and the output terminals were connected to the dipole conductor described above in a physiological saline bath. The battery was activated by dropping the electrodes in the bath, and a signal of amplitude $\sim 2\text{ mV}$ at a frequency of 20 kHz was observed for at least a minute.

Finally, the output terminals of the chip were shorted together, effectively configuring the chip for the 2-terminal operation described above. An output signal was observed, but its amplitude was much weaker, probably because of the decreased effective transmitter dipole length in this configuration. That is, in the 4-terminal configuration, the effective transmit conductor size is determined by the spacing between the battery and dipolar T, which was several centimeters; in the 2-terminal mode, the effective dipole length is reduced to the separation between the Mg and CuI electrodes, which was less than 1 cm. The observed signal was perhaps a few hundred μV , and could be quantified using averaging to overcome an interfering signal amplified by the broadband receiver. More sophisticated detection schemes will have little problem detecting such a signal reliably.

Example 4.

A pill composition as described above prior to ingestion may be composed of two main components, an address generating logic circuit and a signal transmission circuit. The address generation circuit is powered with low current adequate to the required tasks. However, if the voltage supplied to the address

generation circuit changes, the frequency of the oscillator therein will also change. This may produce changes in signal transmission, introduce noise into the transmission, and cause other undesired effects.

For design purposes, it is simpler to power the address generation circuit
5 with a constant voltage. However, in certain embodiments a more complex configuration may be desired. By example, when the transmission starts, the transmitter consumes considerable energy. As a result, the voltage will drop because as more energy is consumed, the voltage of the power source drops. The change in voltage will result in a change of frequency in the oscillator within
10 the address generation circuit.

An example of this challenge in a different area of engineering is when a remote control device is made from a receiver and servos. By contrast, the receiver works permanently, and consumes low current in proportion to the servo which consumes a very large current. The servos work only when a signal is
15 transmitted to the remote site. In that case, the whole system consumes a relatively large amount of power when the servos start to work. When the servo starts to work, the voltage drops, and produces some noise. As a result, the stability of signal transmission is compromised.

In order to avoid this problem, embodiments of the system are powered
20 with two voltage sources. The receivers are powered with one battery, and the servos are powered with another battery. With this configuration, whatever occurs in the servo does not affect the receiver. As such, a more stable remote control results, thereby improving the performance of the complete system.

In one embodiment, a common cathode is provided. There are also two
25 positive electrodes, A1 and A2. In this case, with the battery divided into two parts, one part of the battery will power the address generation circuit, and the other will power the transmission circuit. This configuration provides a stable voltage to the address generation circuit. When the transmitter section of the device is turned on, only the voltage on the transmitter will change, but no
30 change of voltage will occur in the address generation section of the device. Hence, the changes will typically cause a change in signal amplitude, but not in the frequency. As a result, the transition will be more stable, and the frequency of RF transmission will be unaffected, or minimally effected.

The above phenomena are not of concern if there is a big area of battery electrode, because the voltage of the system as a whole will not change. However, in the case of a small battery electrode, the transmitter can potentially lower the voltage of the battery, and there will be a change in voltage over the entire circuitry. If the battery is divided into two parts, the voltage of one battery can be changed while the other will continue to power the address generation circuit with a constant voltage.

A consideration in the design development is how one battery will affect the other. Experiments conducted by some of the present inventors show that a change of load on one battery does not affect the other; i.e., they worked independently. In this experiment, as is shown in **FIG. 23**, two copper iodine anode electrodes were provided with a magnesium electrode as a common cathode. These were connected to a zero-resistance ammeter, and performance was measured. One copper iodine electrode was connected through a 2.5 K Ω resistor, and the other through a 200 K Ω resistor. All the electrodes are submerged in a pH2 HCl solution at about 37°C. The data derived from this experiment is shown in **FIG. 24**. The two copper iodine electrodes work independently of each other.

An ordinary skilled artisan will easily identify different materials and configurations for the above device. The chemistry of this copper iodine and various manners of preparation will be understood or quickly developed.

The surface preparation before the copper iodine is forming is of interest. One approach is to use copper wire embedded in epoxy. This can be plated with electrolytic copper. After the copper is polarized in solution of potassium iodide, copper iodine is formed on the tip of the electrode. Copper iodine can also be formed by chemically deposition. Other means are also available.

10 μm is a typical range for thickness of copper iodide to produce an adequate amount of electricity to accomplish the activity of the device for a 15 minute period. If less thickness is employed, the transmission will last a shorter time. Thus, the thickness of copper iodide is determined by the time required to produce electricity to provide the results needed for a particular application. For several seconds of transmission, less than 1 μm of copper iodide would be adequate. For one microsecond of transmission, a few nanometers of copper

iodine thickness, such as in the range of about 10-100 nanometers, more specifically, about 20-50 nanometers is sufficient.

5 It is to be understood that this invention is not limited to particular embodiments described, as such may vary. It is also to be understood that the terminology used herein is for the purpose of describing particular embodiments only, and is not intended to be limiting, since the scope of the present invention will be limited only by the appended claims.

10 Where a range of values is provided, it is understood that each intervening value, to the tenth of the unit of the lower limit unless the context clearly dictates otherwise, between the upper and lower limit of that range and any other stated or intervening value in that stated range, is encompassed within the invention. The upper and lower limits of these smaller ranges may independently be included in the smaller ranges and are also encompassed within the invention, 15 subject to any specifically excluded limit in the stated range. Where the stated range includes one or both of the limits, ranges excluding either or both of those included limits are also included in the invention.

Unless defined otherwise, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the 20 art to which this invention belongs. Although any methods and materials similar or equivalent to those described herein can also be used in the practice or testing of the present invention, representative illustrative methods and materials are now described.

25

The citation of any publication is for its disclosure prior to the filing date and should not be construed 30 as an admission that the present invention is not entitled to antedate such publication by virtue of prior invention. Further, the dates of publication provided may be different from the actual publication dates which may need to be independently confirmed.

It is further noted that the claims may be drafted to exclude any optional element. As such, this statement is intended to serve as antecedent
5 basis for use of such exclusive terminology as "solely," "only" and the like in connection with the recitation of claim elements, or use of a "negative" limitation.

As will be apparent to those of skill in the art upon reading this disclosure, each of the individual embodiments described and illustrated herein has discrete components and features which may be readily separated from or combined with
10 the features of any of the other several embodiments.

Any recited method can be carried out in the order of events recited or in any other order which is logically possible.

Although the foregoing invention has been described in some detail by way of illustration and example for purposes of clarity of understanding, it is
15 readily apparent to those of ordinary skill in the art in light of the teachings of this invention that certain changes and modifications may be made thereto.

Accordingly, the preceding merely illustrates the principles of the invention. It will be appreciated that those skilled in the art will be able to devise various
20 arrangements which, although not explicitly described or shown herein, embody the principles of the invention.

Furthermore, all examples and conditional language recited herein are principally intended to aid the reader in understanding the principles of the invention and the concepts contributed by the inventors to furthering the art, and are to be
25 construed as being without limitation to such specifically recited examples and conditions. Moreover, all statements herein reciting principles, aspects, and embodiments of the invention as well as specific examples thereof, are intended to encompass both structural and functional equivalents thereof. Additionally, it is intended that such equivalents include both currently known equivalents and
30 equivalents developed in the future, i.e., any elements developed that perform the same function, regardless of structure. The scope of the present invention, therefore, is not intended to be limited to the exemplary embodiments shown and described herein.

What is claimed is:

1. A receiver comprising a receiver element configured to receive a conductively transmitted signal emitted by an identifier that conductively transmits a signal upon contact with an internal target physiological site, wherein the receiver comprises a data storage element, and wherein the data storage element is configured to store data comprising at least one of time, date and identity of an ingested composition.
2. The receiver according to claim 1, wherein the conductively transmitted signal has a frequency that ranges from 1 KHz to 100 MHz.
3. The receiver according to claim 2, wherein the conductively transmitted signal has a frequency that ranges from 1 KHz to 70 KHz.
4. The receiver according to claim 2, wherein the conductively transmitted signal has a frequency that ranges from: 30 KHz to 300 KHz; 160 KHz to 190 KHz or 3 KHz to 30 KHz.
5. The receiver according to claim 1, wherein the receiver element comprises a receiving antenna configured to detect potential differences in a body.
6. The receiver according to claim 5, wherein the receiving antenna comprises two electrodes spaced apart from each other at a distance sufficient to detect a differential voltage.
7. The receiver according to claim 1, wherein the receiver comprises an amplifier.
8. The receiver according to claim 1, wherein the receiver comprises a filter.
9. The receiver according to claim 1, wherein the receiver comprises a demodulator.
10. The receiver according to claim 1, wherein the receiver is configured to retransmit data to a separate external device.
11. The receiver according to claim 10, wherein the receiver comprises RF circuitry and is configured to retransmit data to a separate external device by using an RF communication protocol.

12. The receiver according to claim 1, wherein the receiver is configured as an in vivo receiver.

13. The receiver according to claim 1, wherein the receiver is configured as an ex vivo receiver.

14. The receiver according to claim 1, wherein the receiver comprises a physiological sensor.

15. A receiver comprising:

a receiver element comprising two electrodes spaced apart from each other at a distance sufficient to detect a differential voltage in a body;

a data storage element; an amplifier; and

a demodulator;

wherein the receiver is configured to retransmit data to a separate external device, and wherein the data storage element is configured to store data comprising at least one of time, date and identity of an ingested composition.

16. The receiver according to claim 15, wherein the receiver is configured as an in vivo receiver.

17. The receiver according to claim 15, wherein the receiver is configured as an ex vivo receiver.

18. A system comprising:

an identifier that conductively transmits a signal upon contact with an internal target physiological site; and

a receiver comprising a receiver element configured to receive a conductively transmitted signal emitted by the identifier and a data storage element configured to store data comprising at least one of time, date and identity of an ingested composition.

19. The system according to claim 18, wherein the conductively transmitted signal has a frequency that ranges from 1 KHz to 100 MHz.

20. The system according to claim 18, wherein the receiver element comprises a receiving antenna configured to detect potential differences in a body.

21. The system according to claim 20, wherein the receiving antenna comprises two electrodes spaced apart from each other at a distance sufficient to detect a differential voltage.

22. The system according to claim 18, wherein the receiver comprises an amplifier.

23. The system according to claim 18, wherein the receiver comprises a demodulator.

24. The receiver according to claim 18, wherein the receiver is configured to retransmit data to a separate external device.

25. A method comprising receiving a signal at a receiver comprising a receiver element configured to receive a conductively transmitted signal emitted by an identifier that conductively transmits a signal upon contact with an internal target physiological site, wherein the receiver further comprises a data storage element, and wherein the method further comprises storing, at the data storage element, at least one of time, date and identity of an ingested composition.

26. The method according to claim 25, wherein the signal is a conductively transmitted signal.

27. The method according to claim 26, wherein the conductively transmitted signal has a frequency that ranges from 1 KHz to 100 MHz.

28. The method according to claim 25, wherein the receiver element comprises a receiving antenna configured to detect potential differences in a body.

29. The method according to claim 28, wherein the receiving antenna comprises two electrodes spaced apart from each other at a distance sufficient to detect a differential voltage.

30. The method according to claim 25, wherein the receiver comprises an amplifier.

31. The method according to claim 25, wherein the receiver comprises a demodulator.

32. The method according to claim 25, wherein the receiver is configured to retransmit data to a separate external device.

33. The method according to claim 32, wherein the method further comprises transmitting a signal from the receiver to the separate external device.

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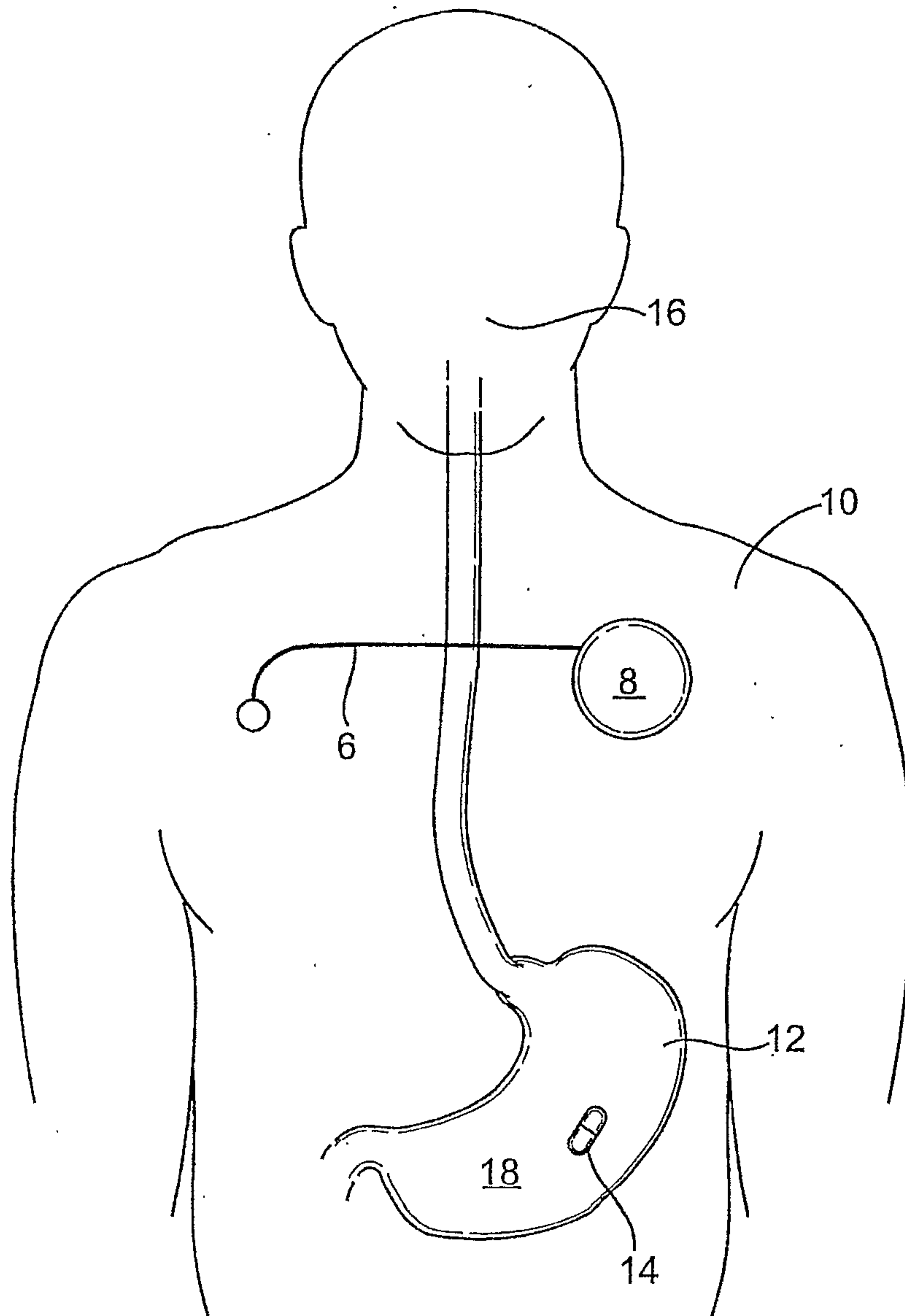


FIG. 1

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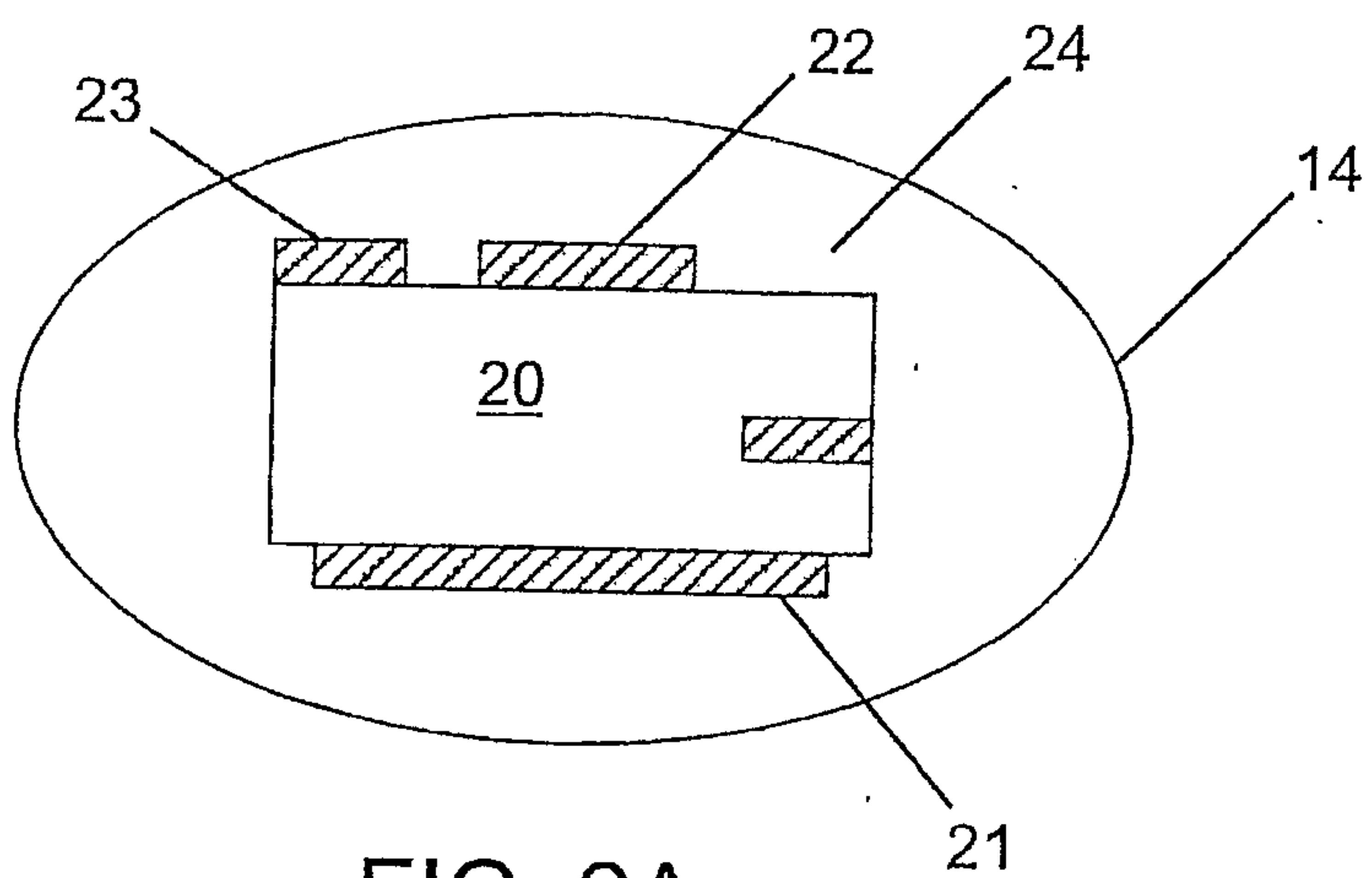


FIG. 2A

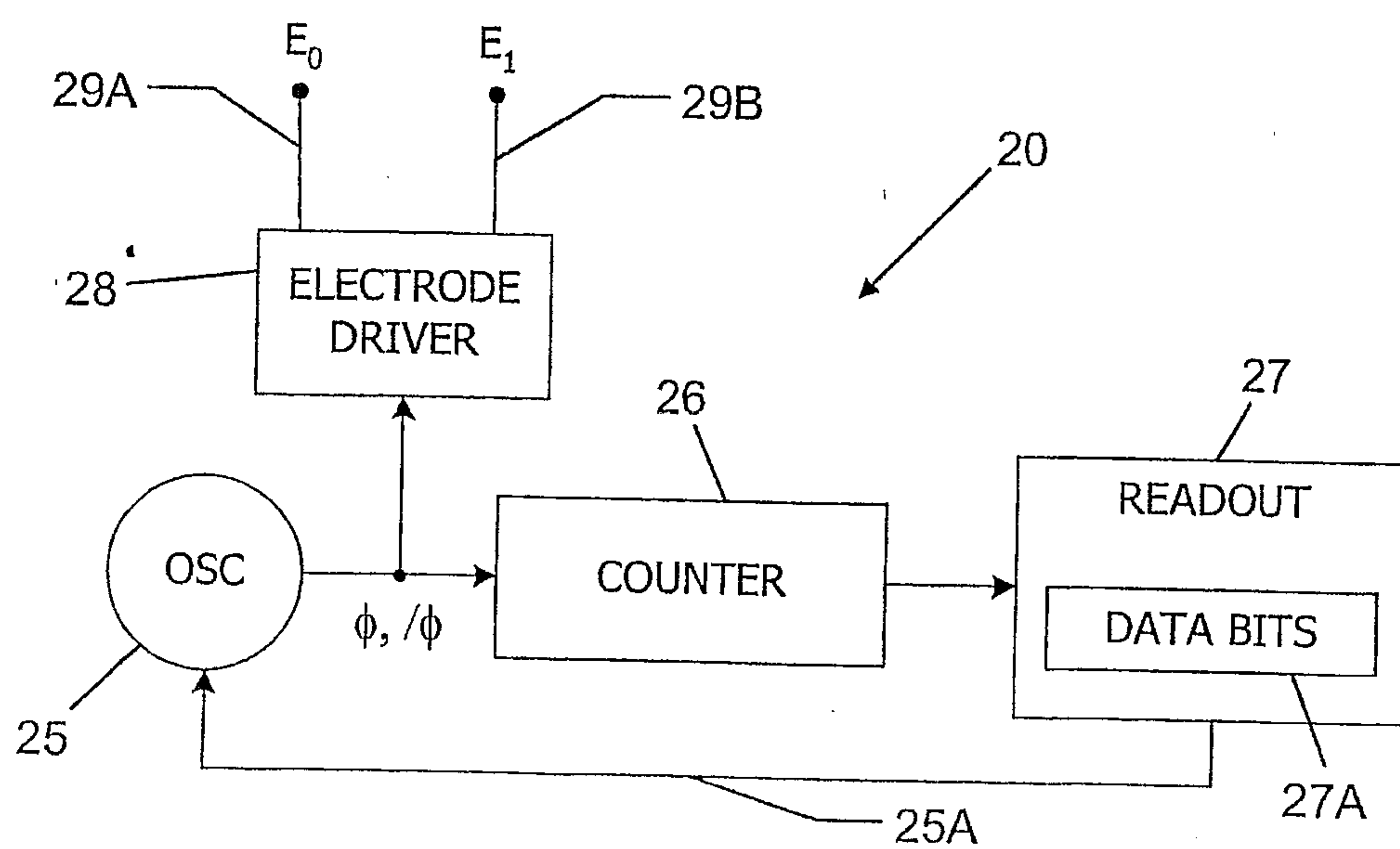


FIG. 2B

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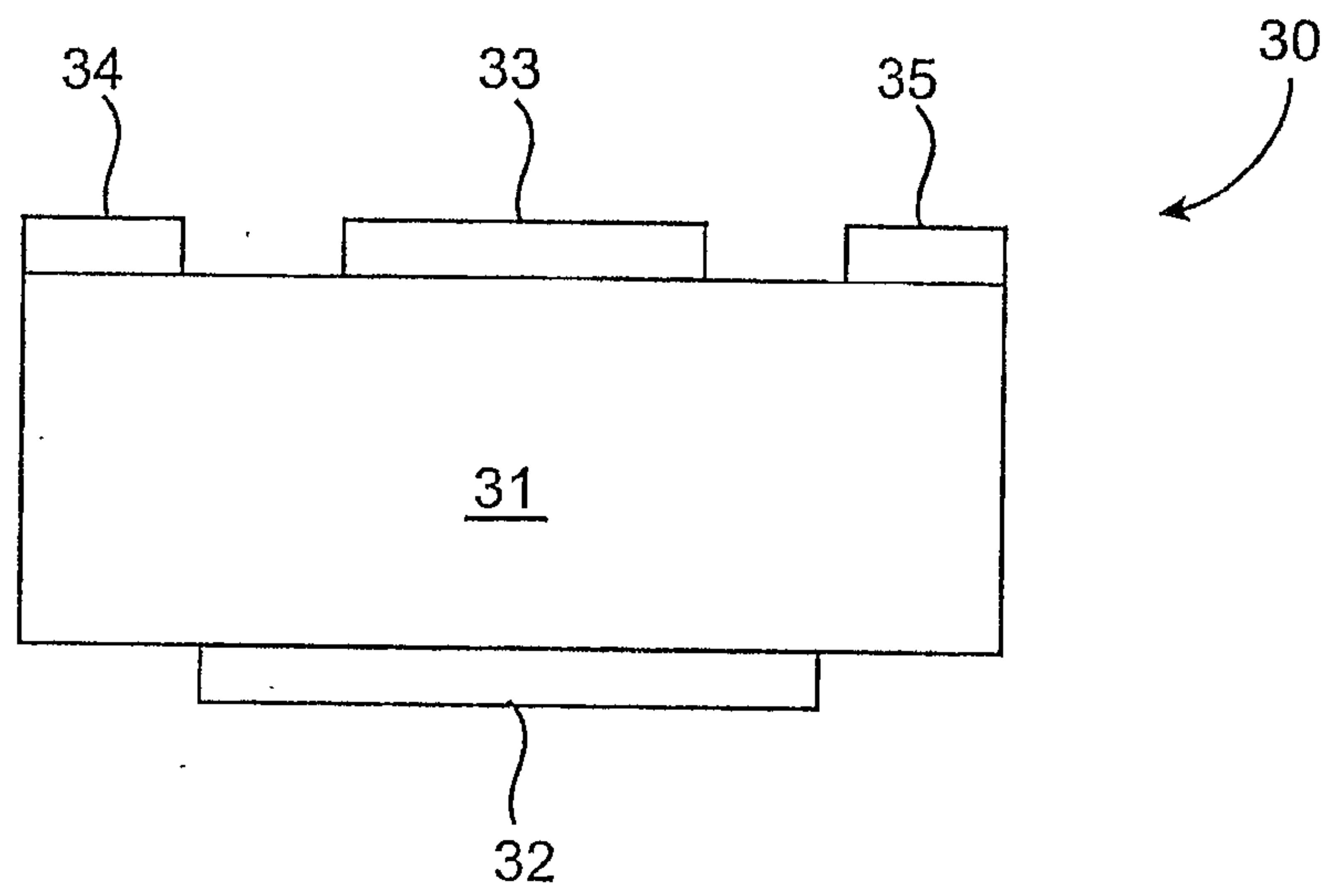


FIG. 3A

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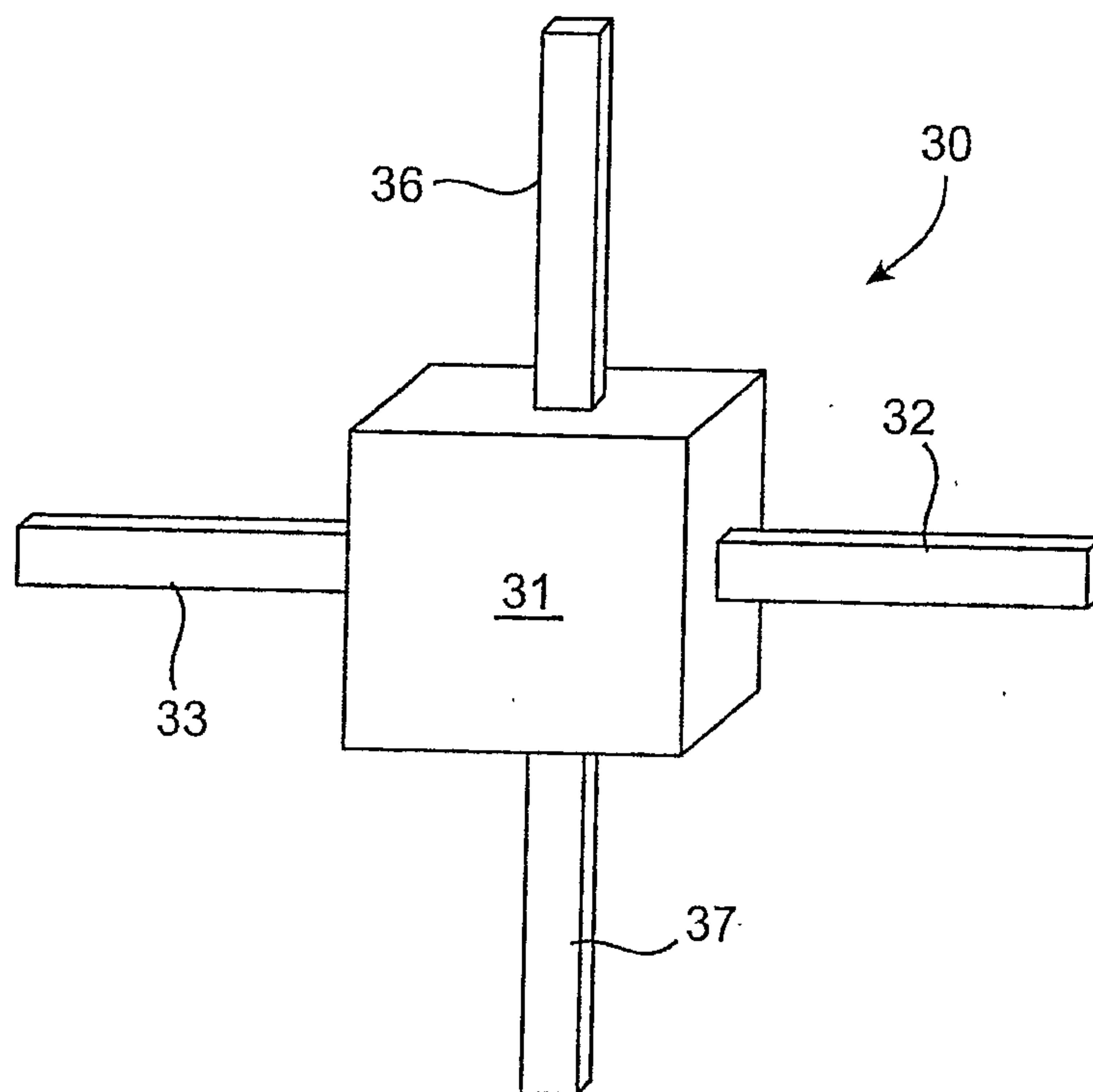


FIG. 3B

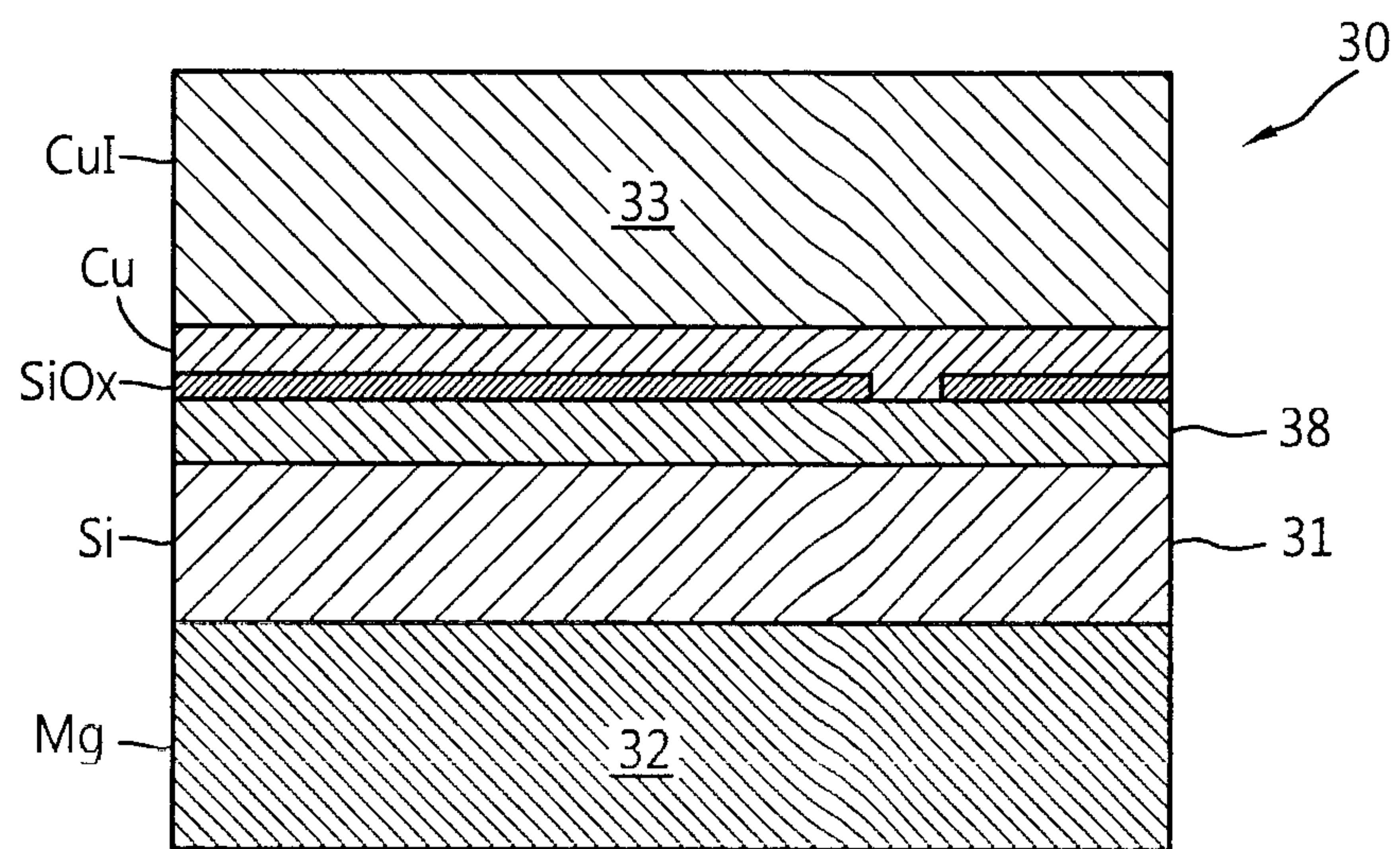


FIG. 3C

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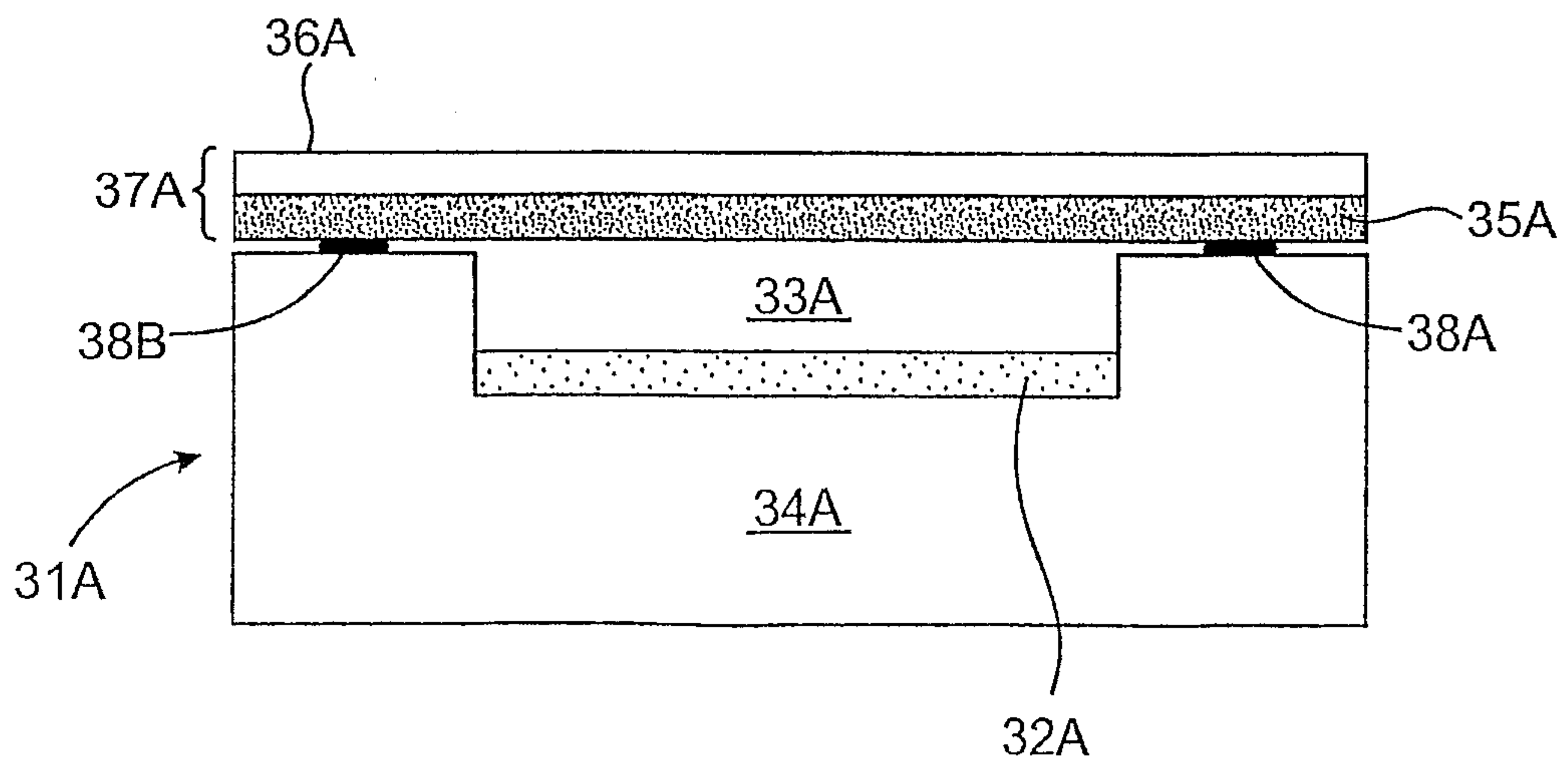
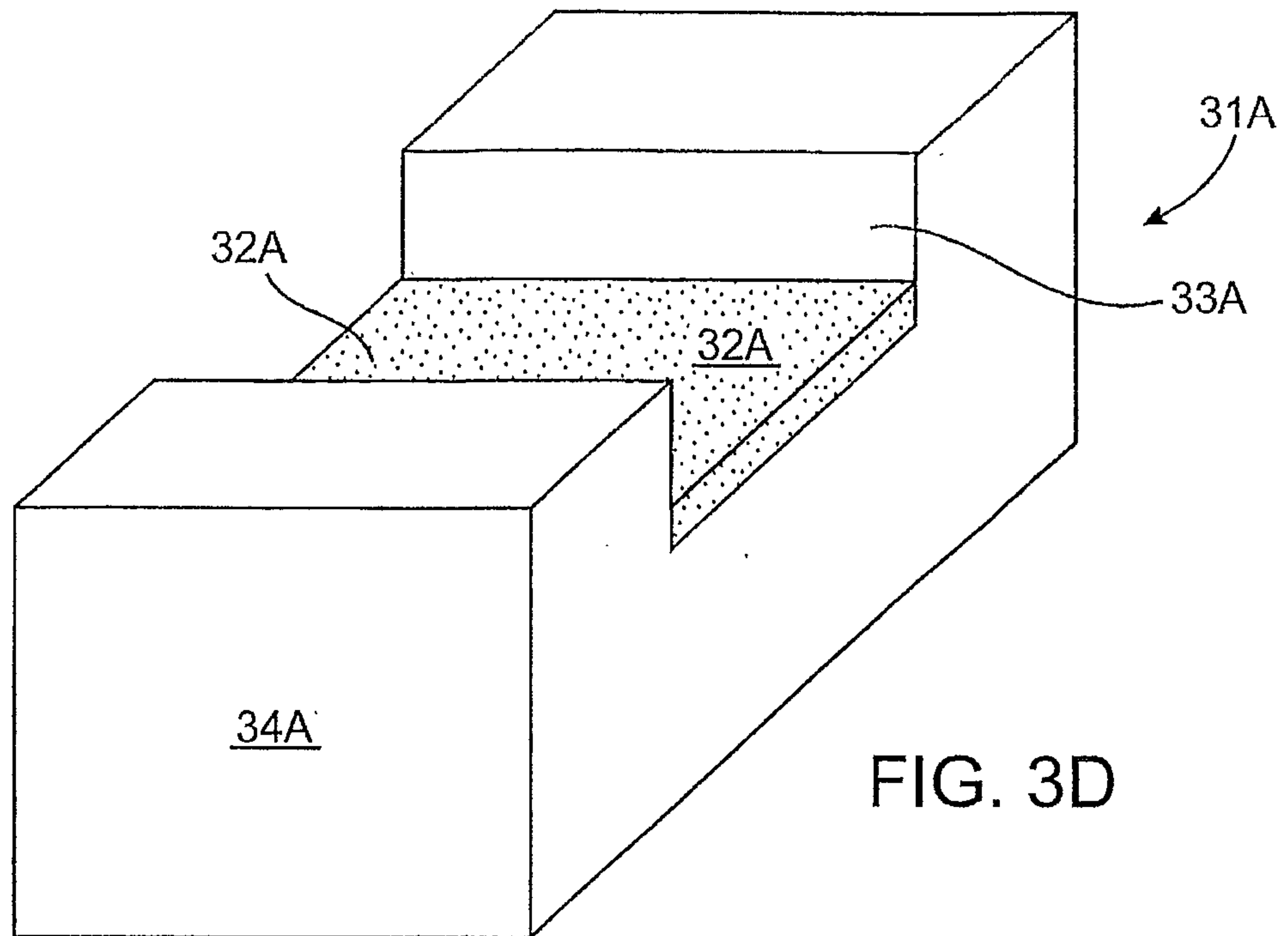


FIG. 3E

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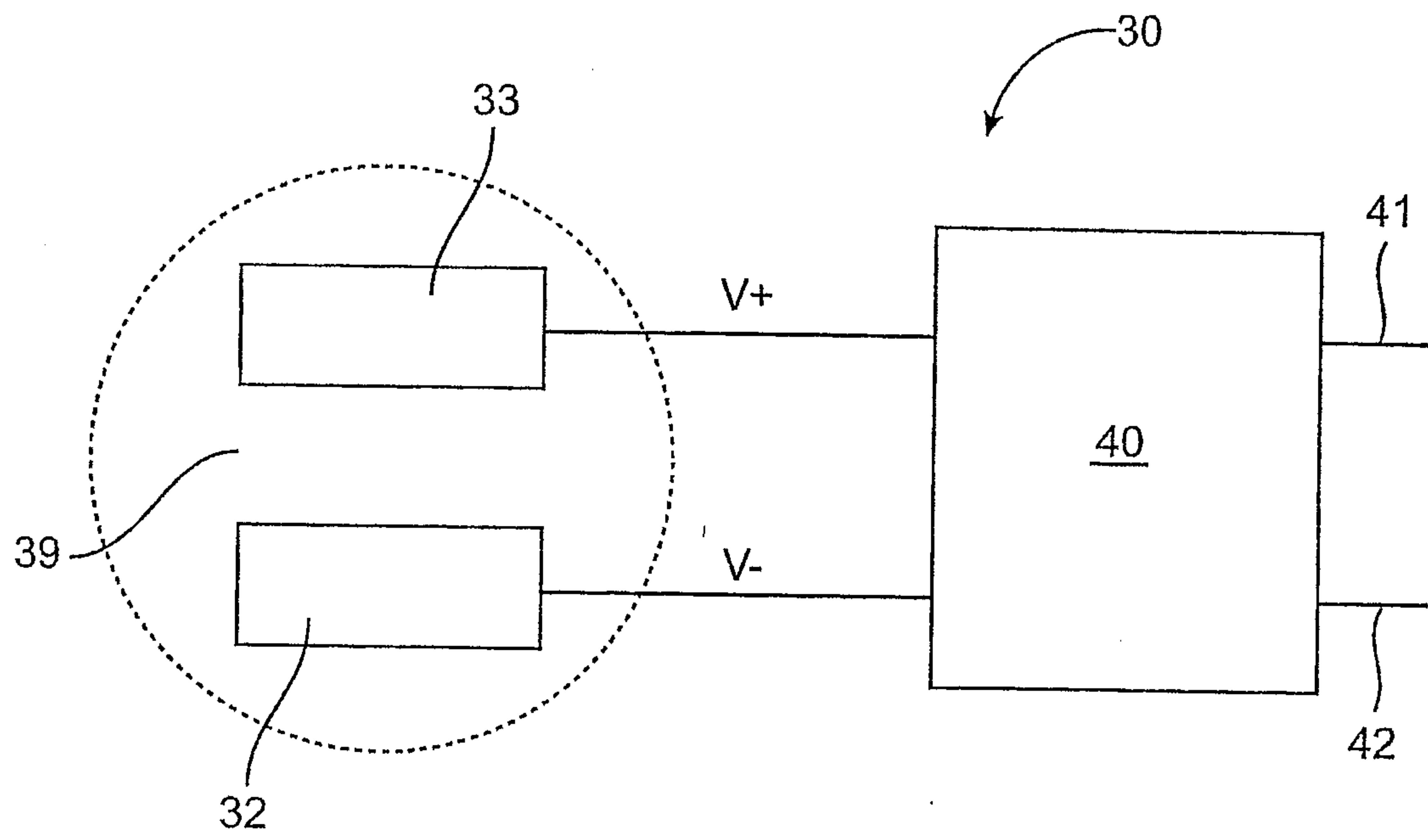


FIG. 4

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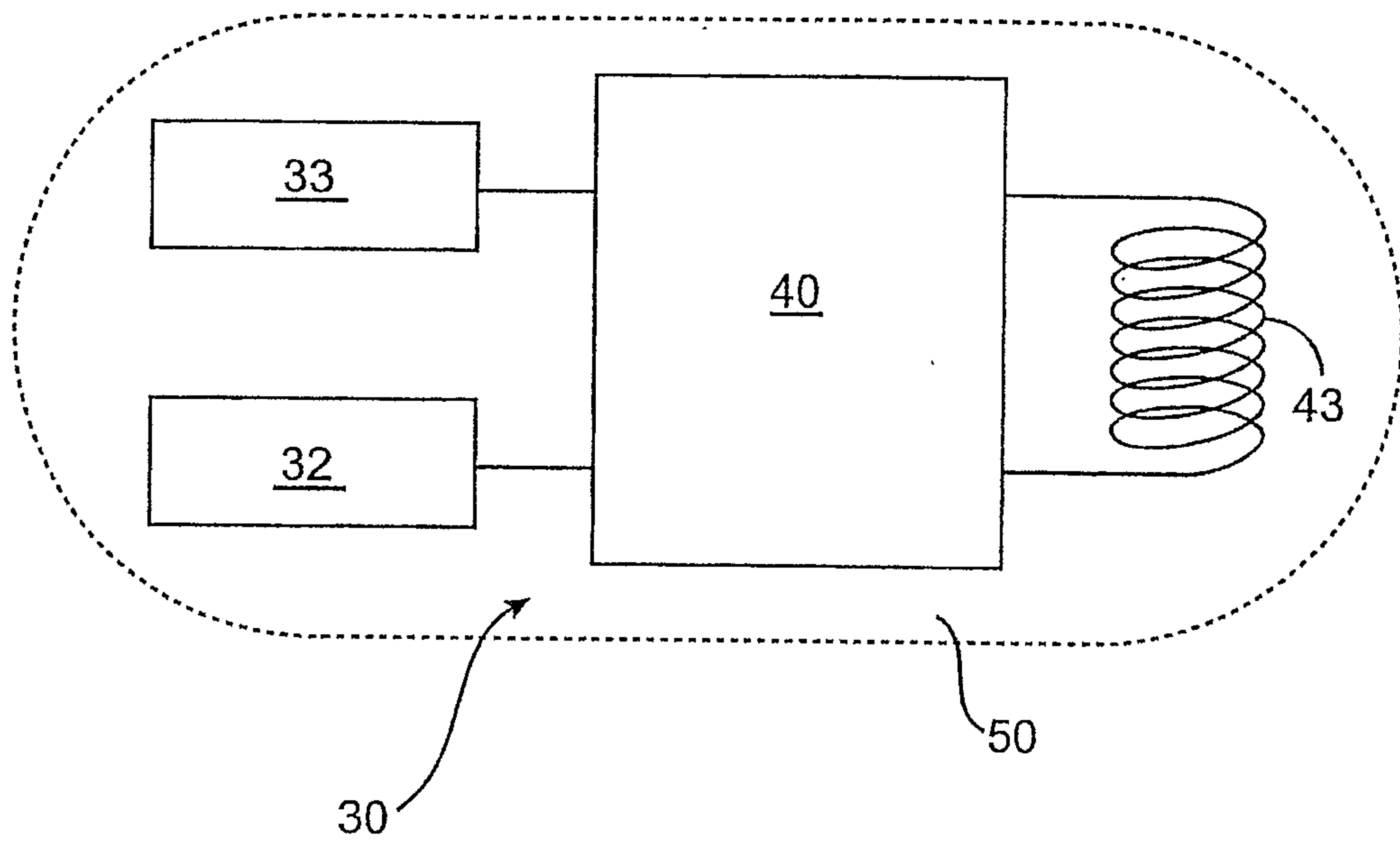


FIG. 5

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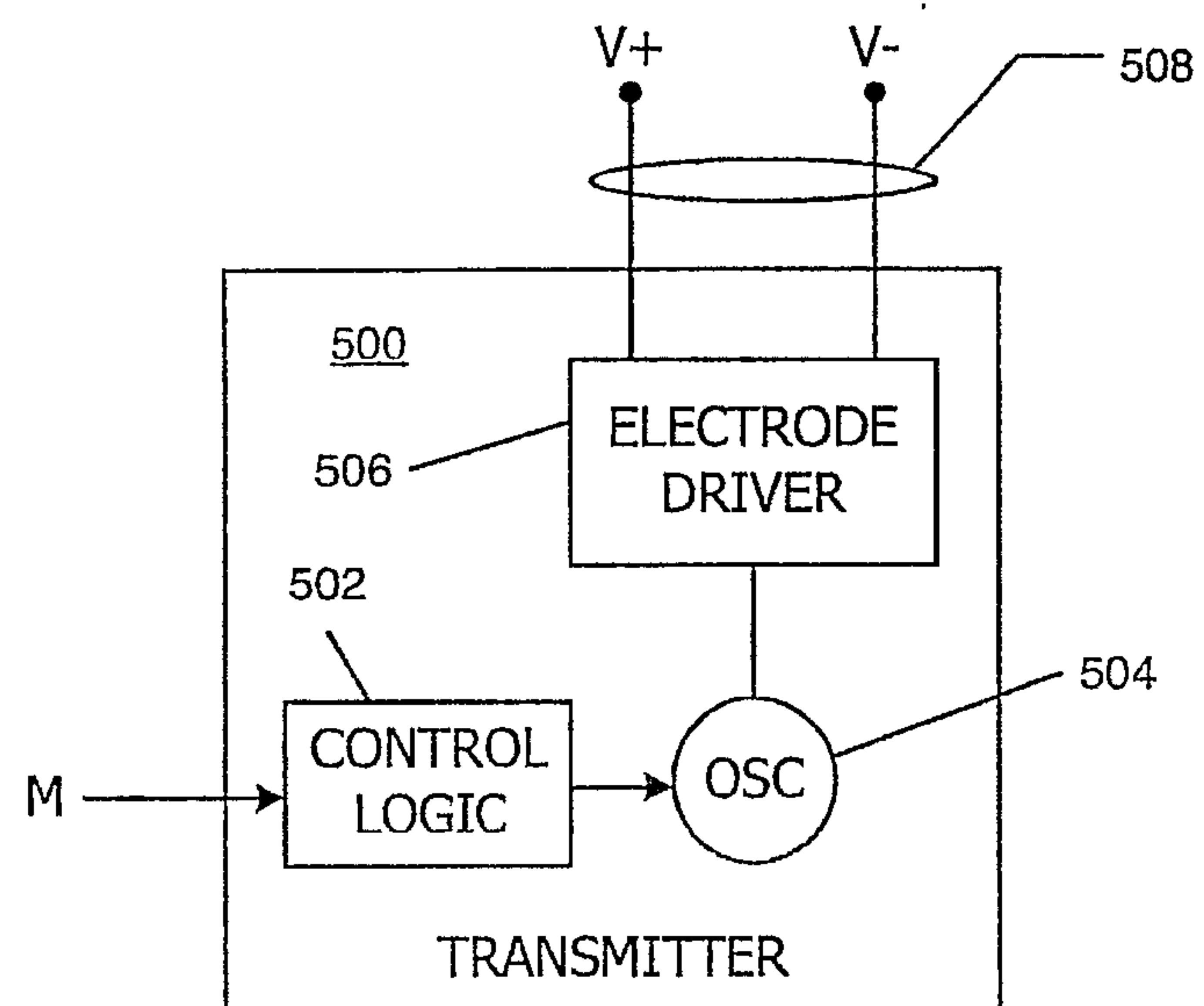


FIG. 6A

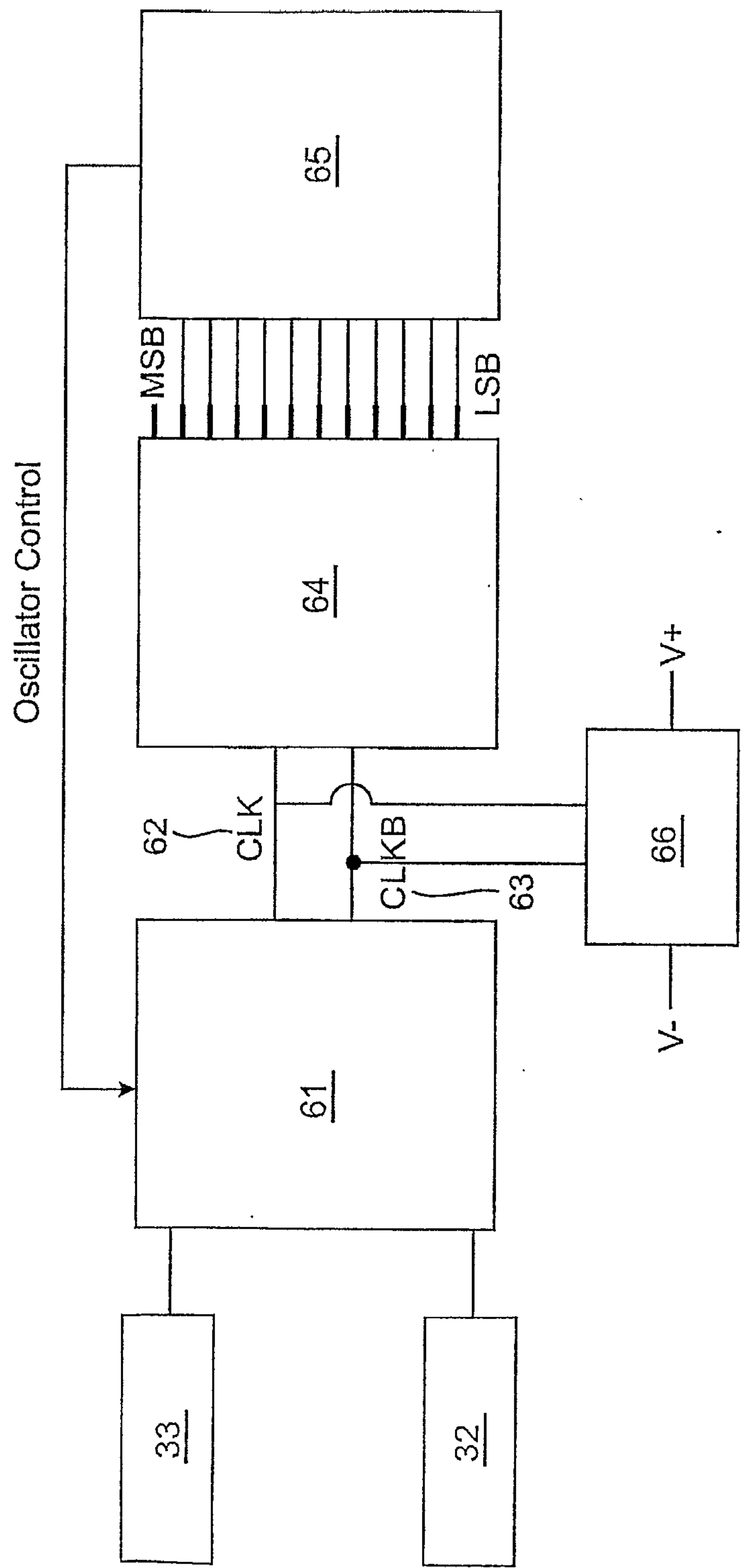


FIG. 6B

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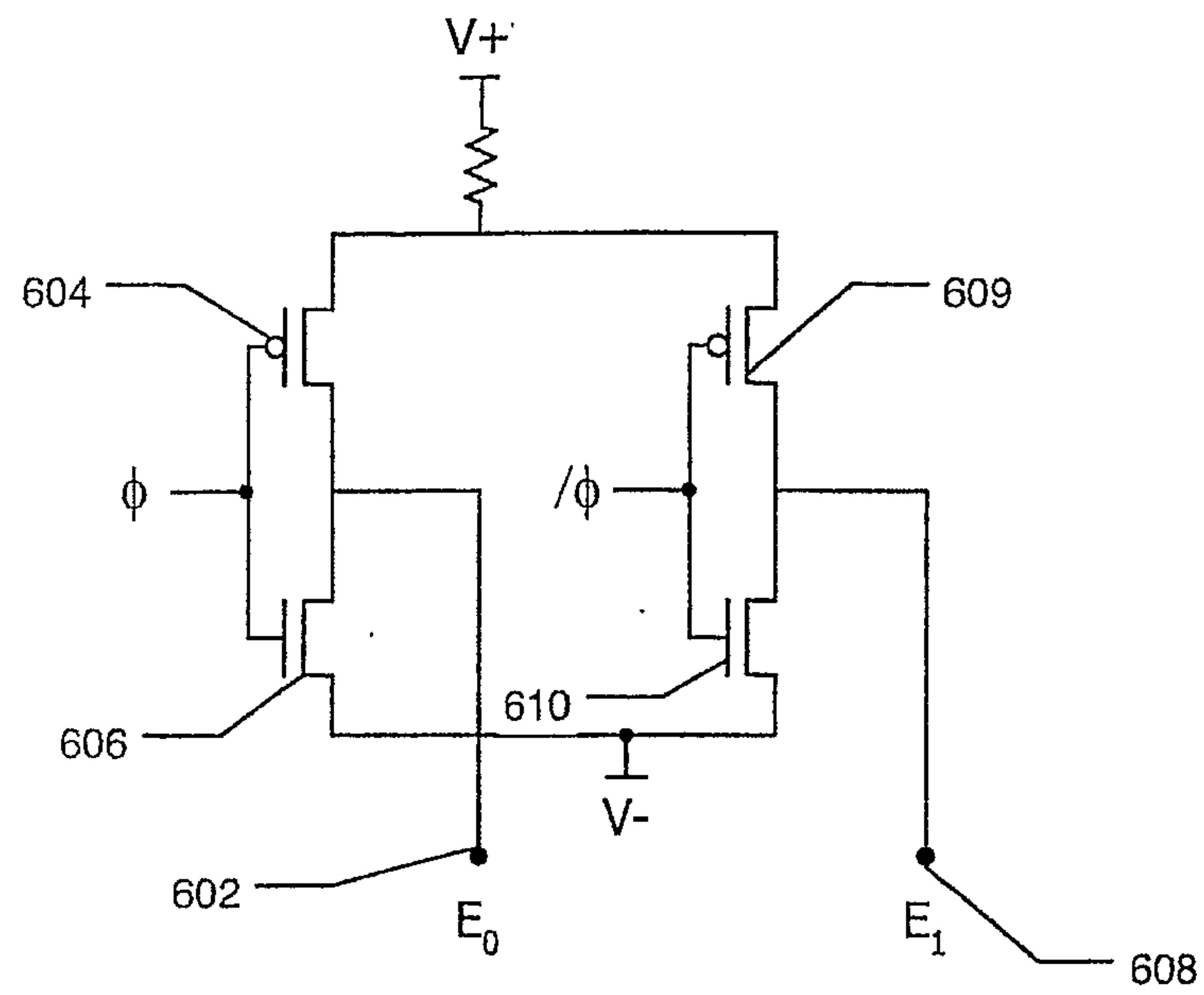


FIG. 6C

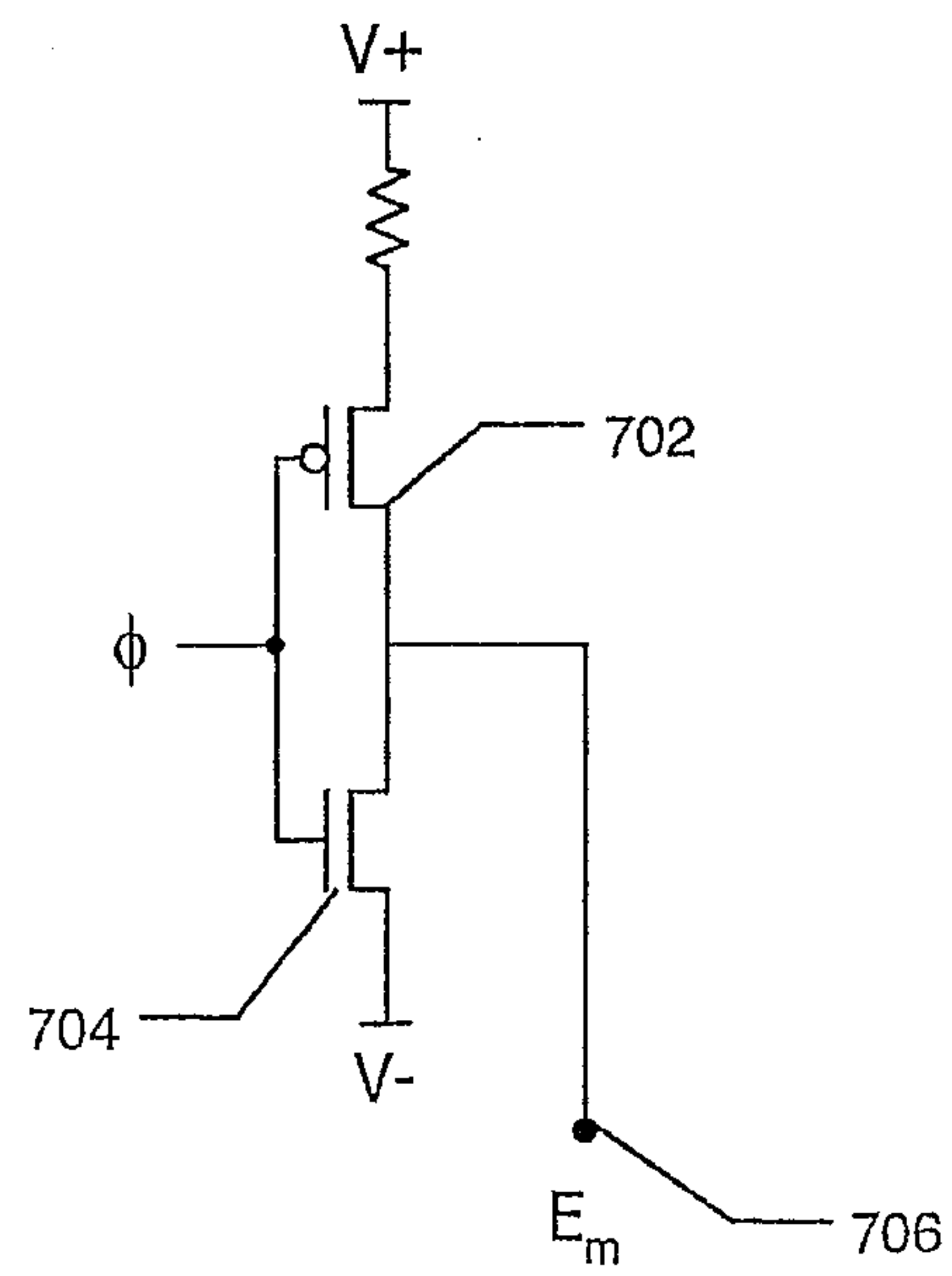


FIG. 6D

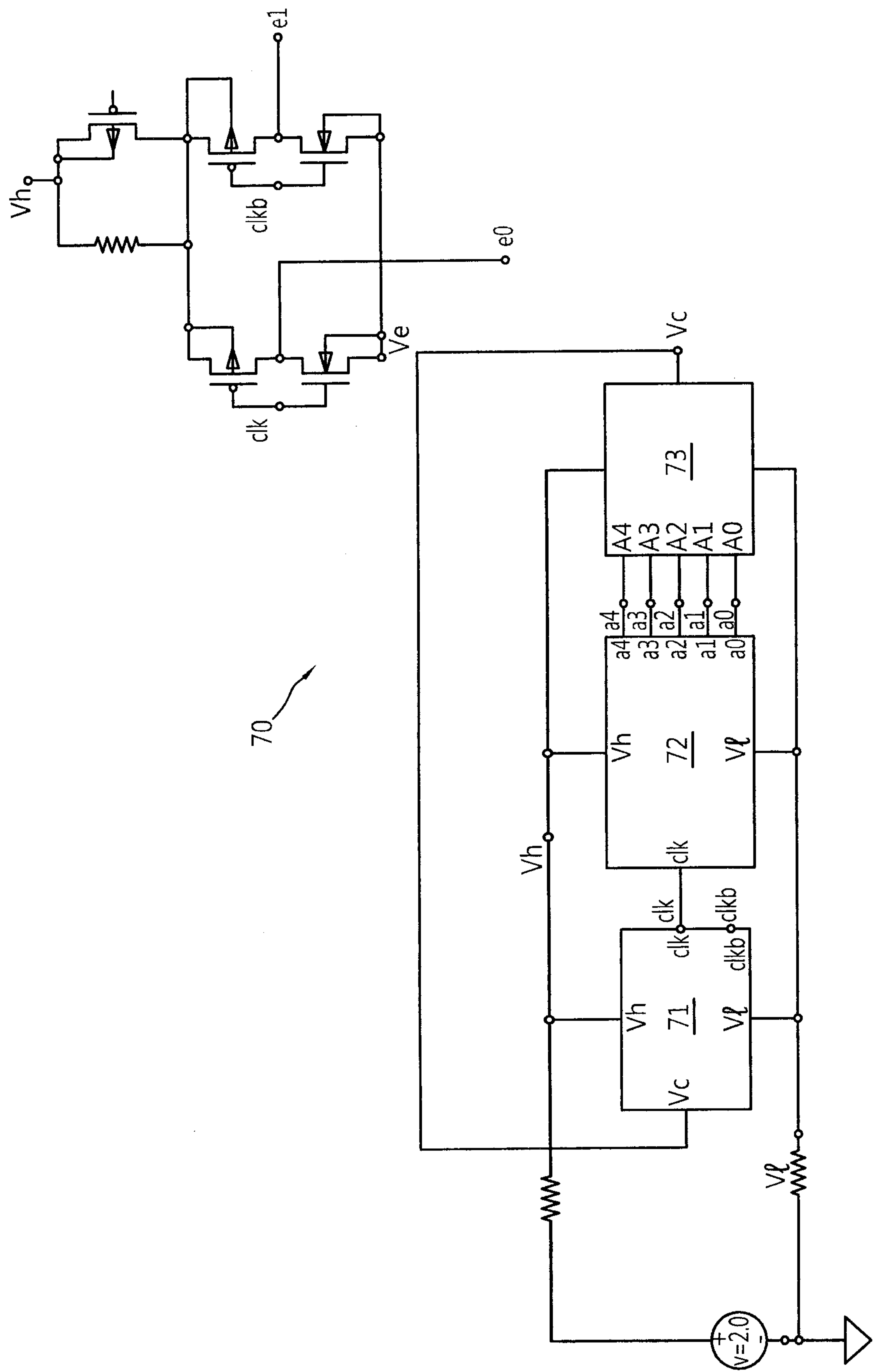


FIG. 7

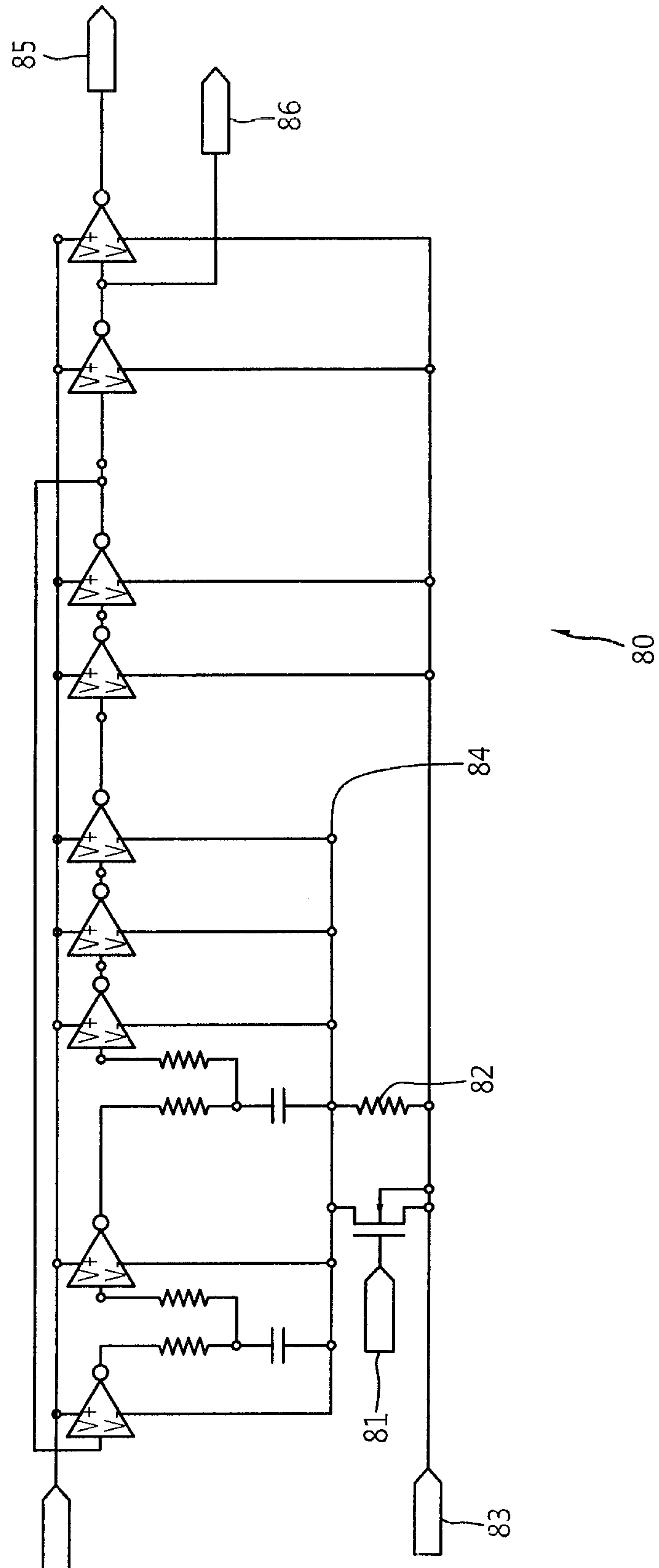


FIG. 8

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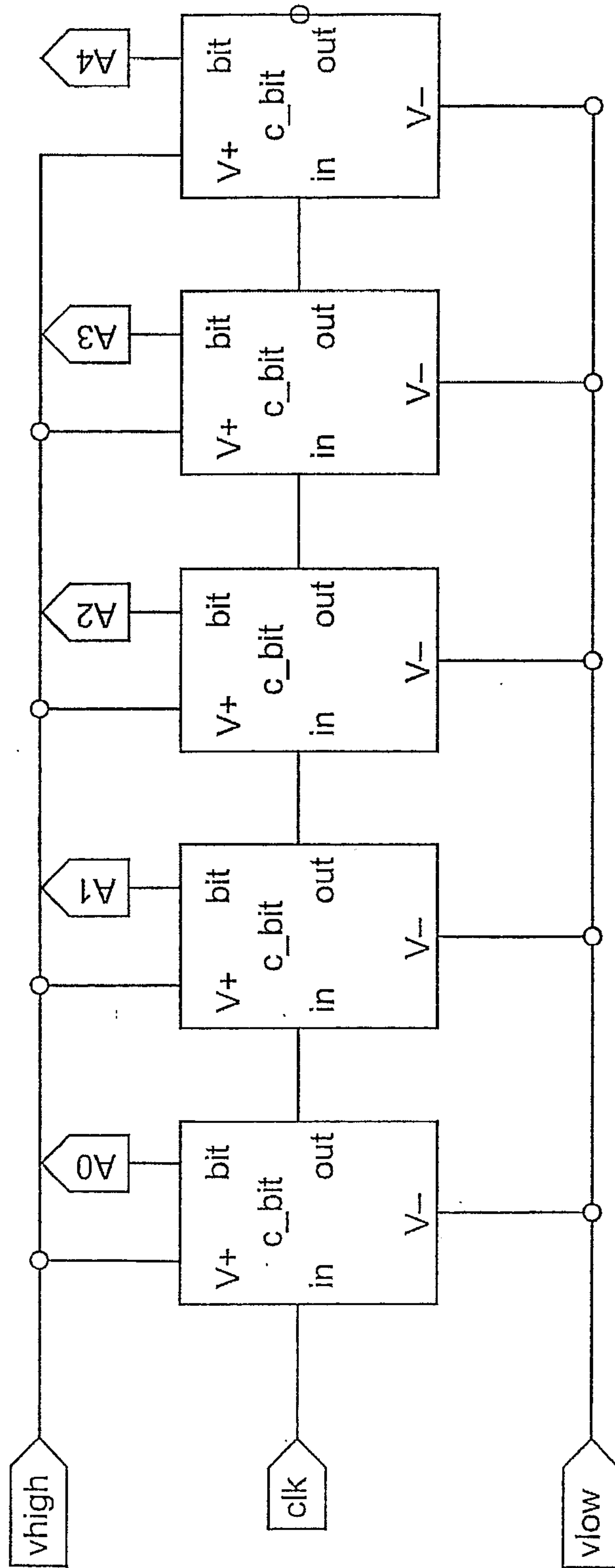


FIG. 9

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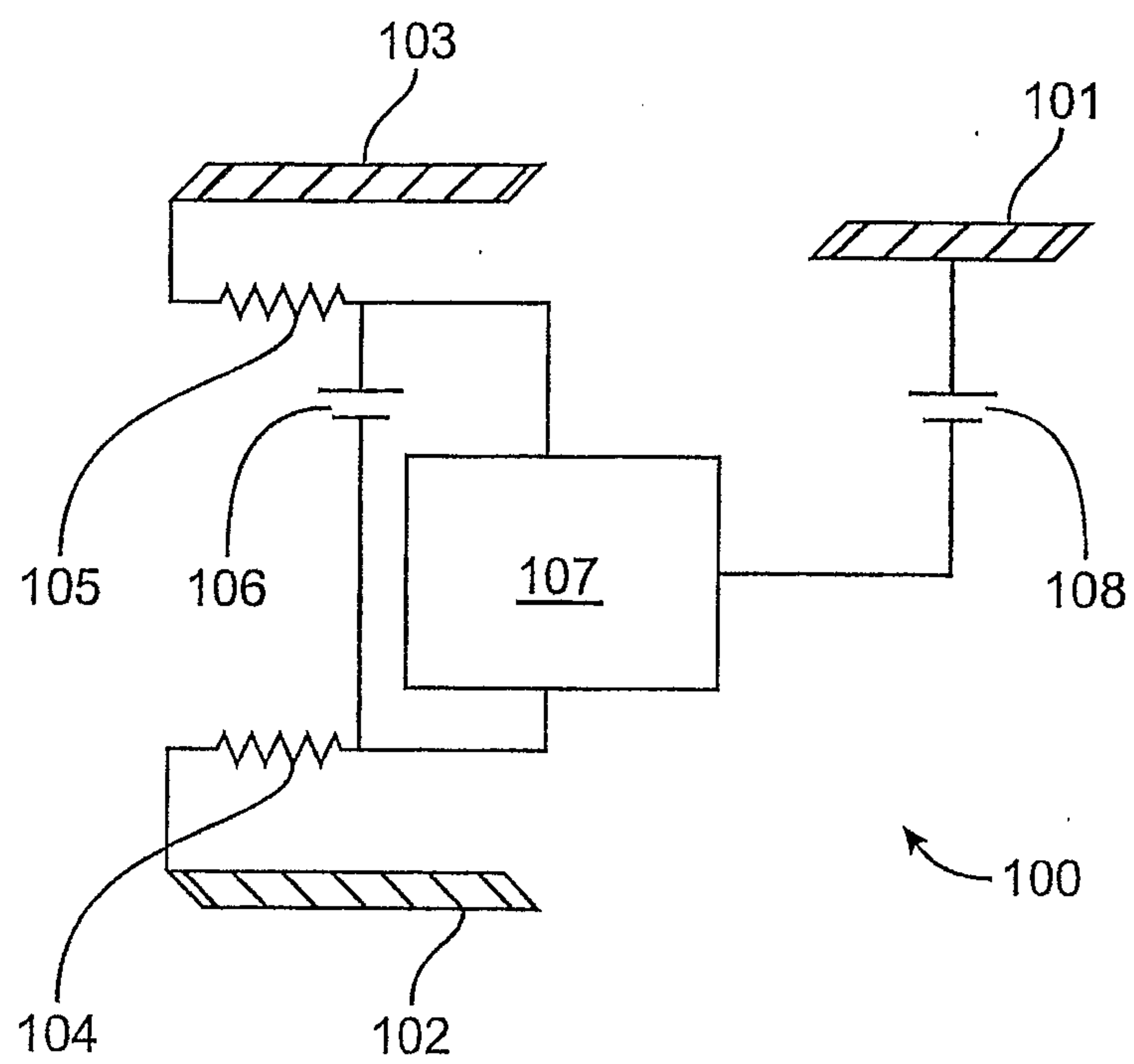


FIG. 10

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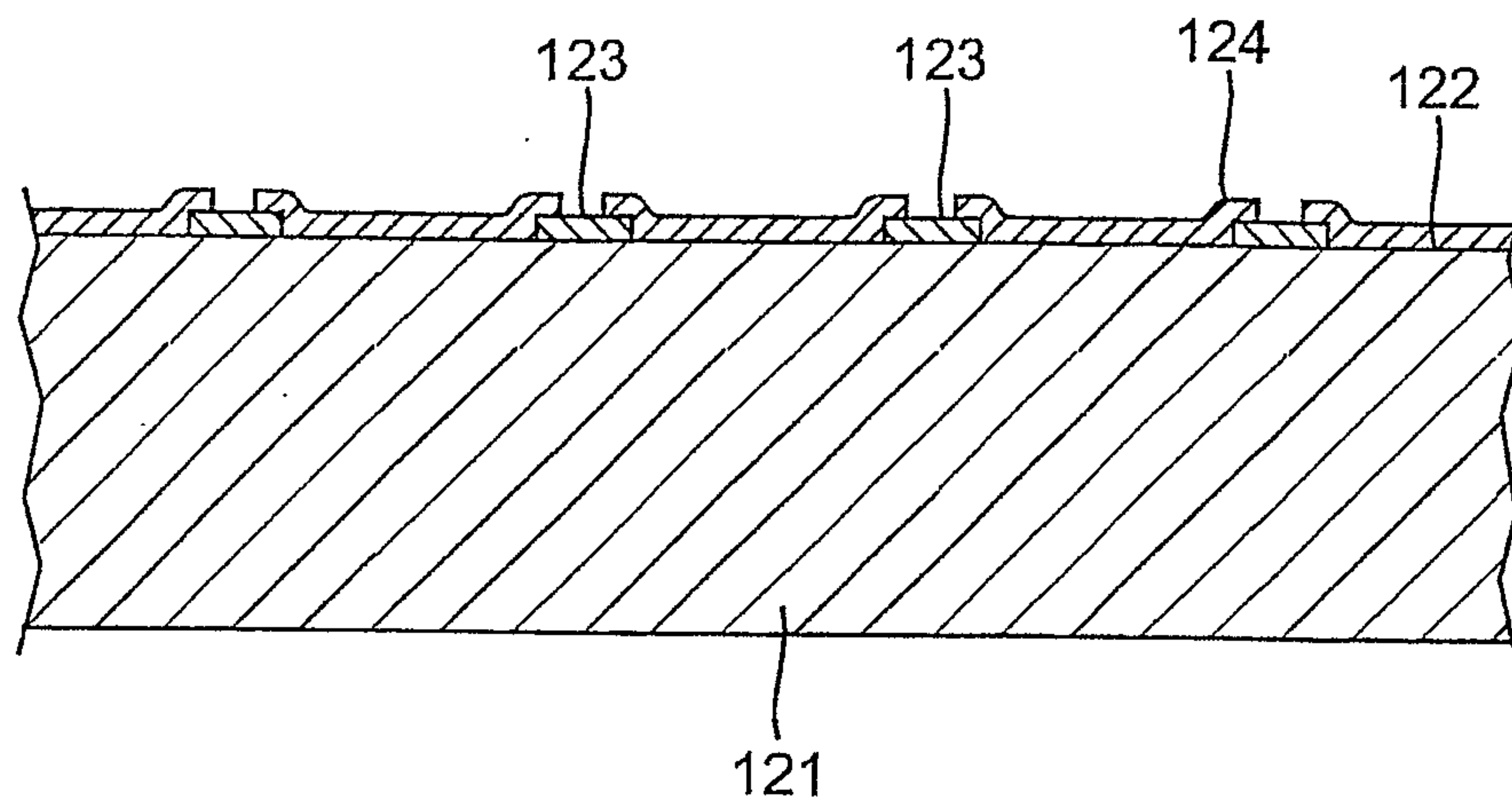


FIG. 11A

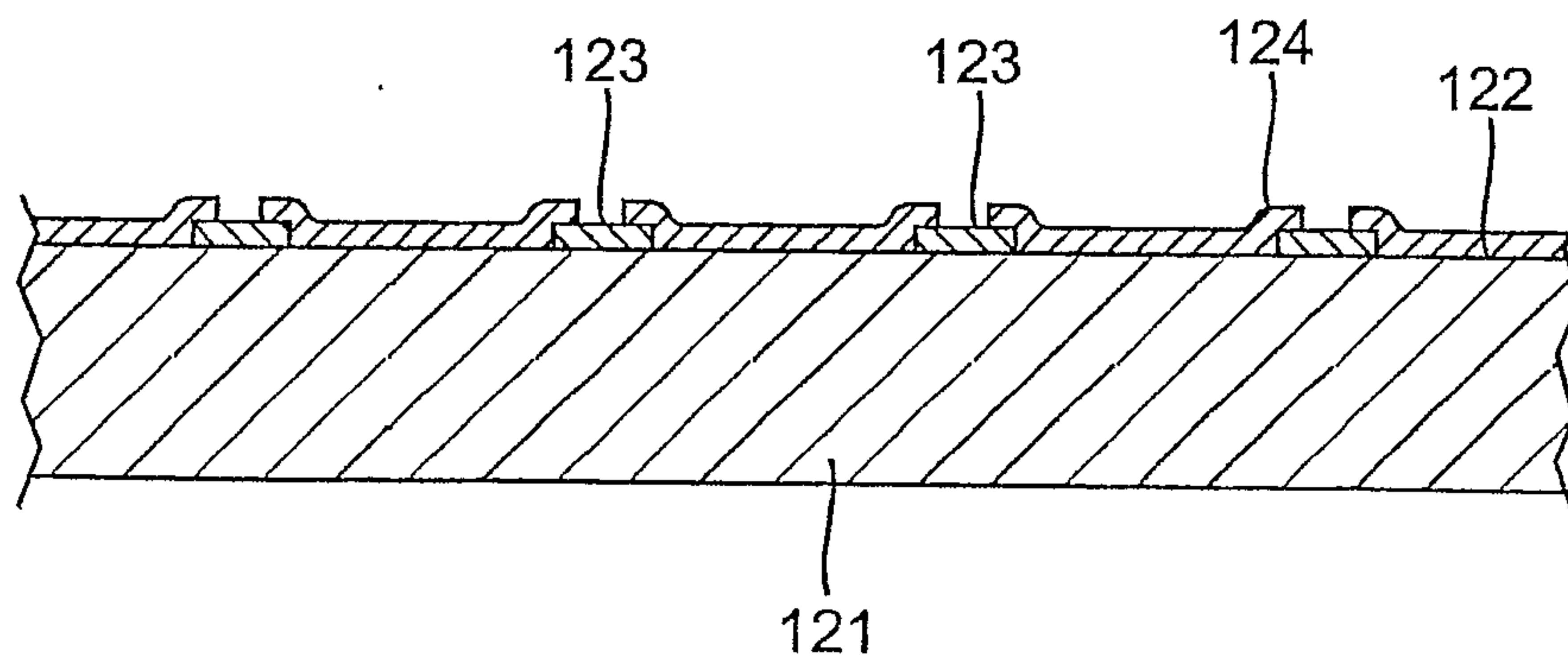


FIG. 11B

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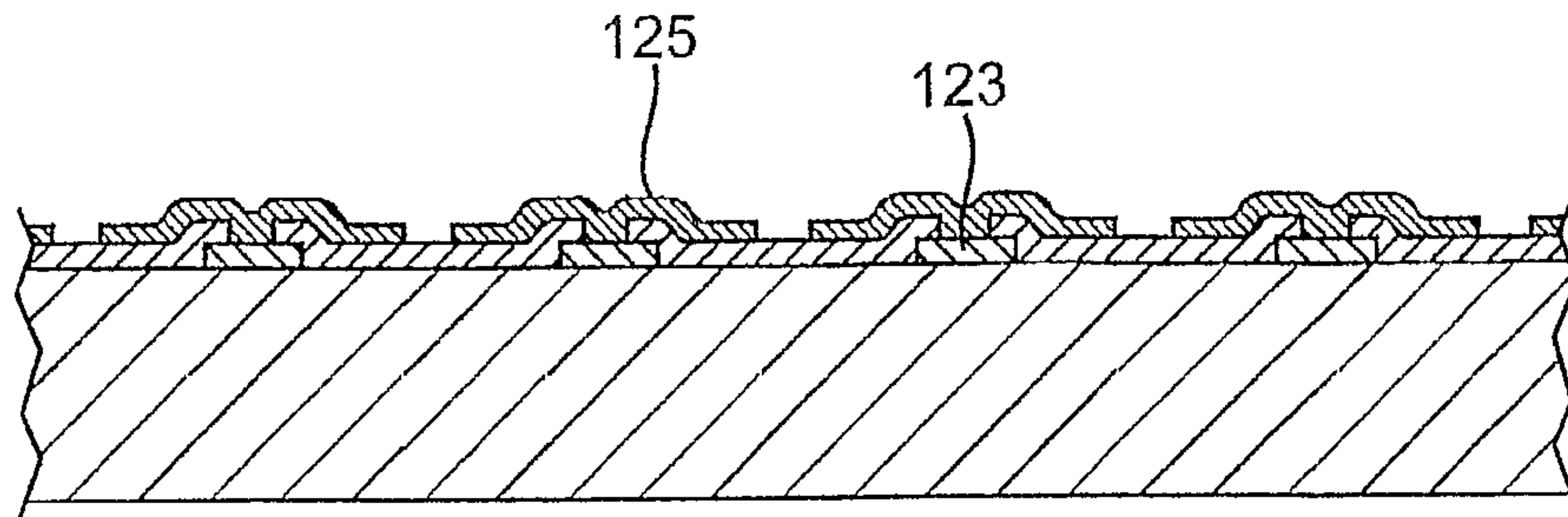


FIG. 12A

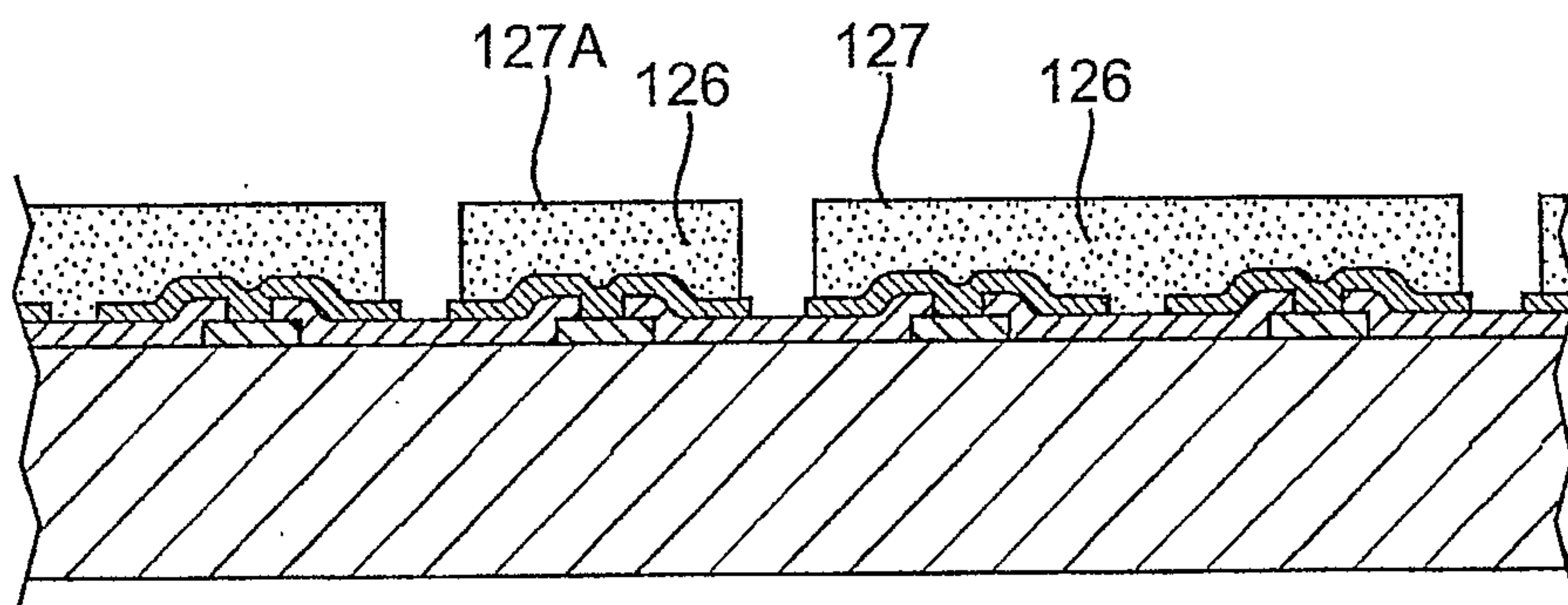


FIG. 12B

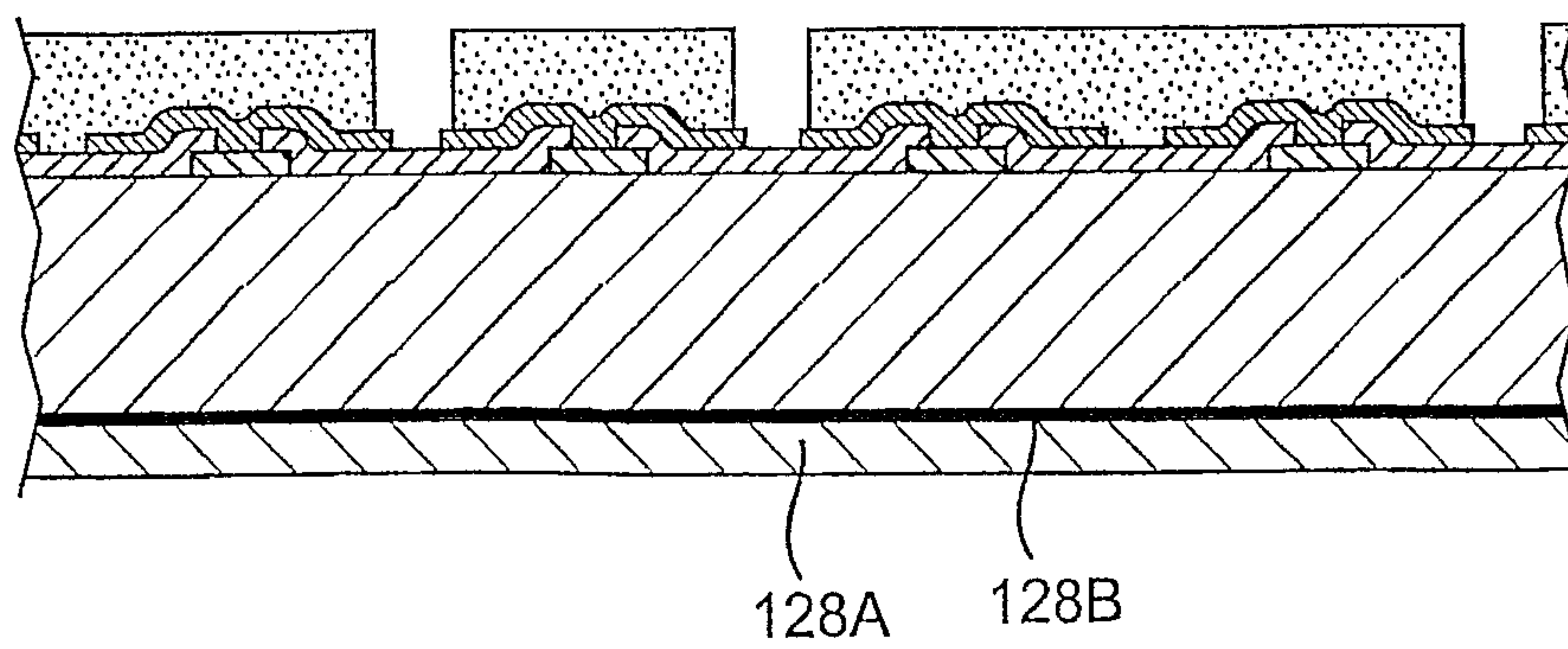


FIG. 12C

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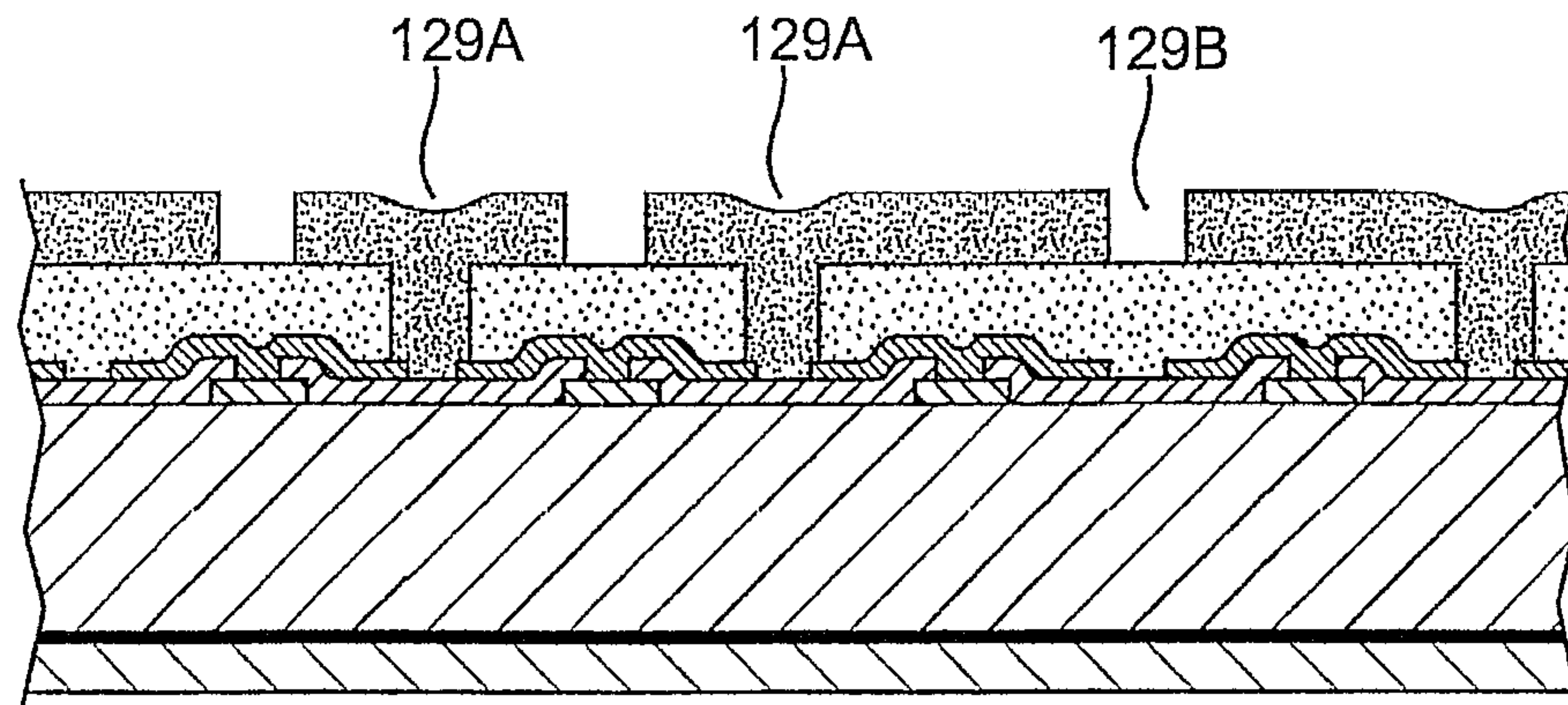


FIG. 13A

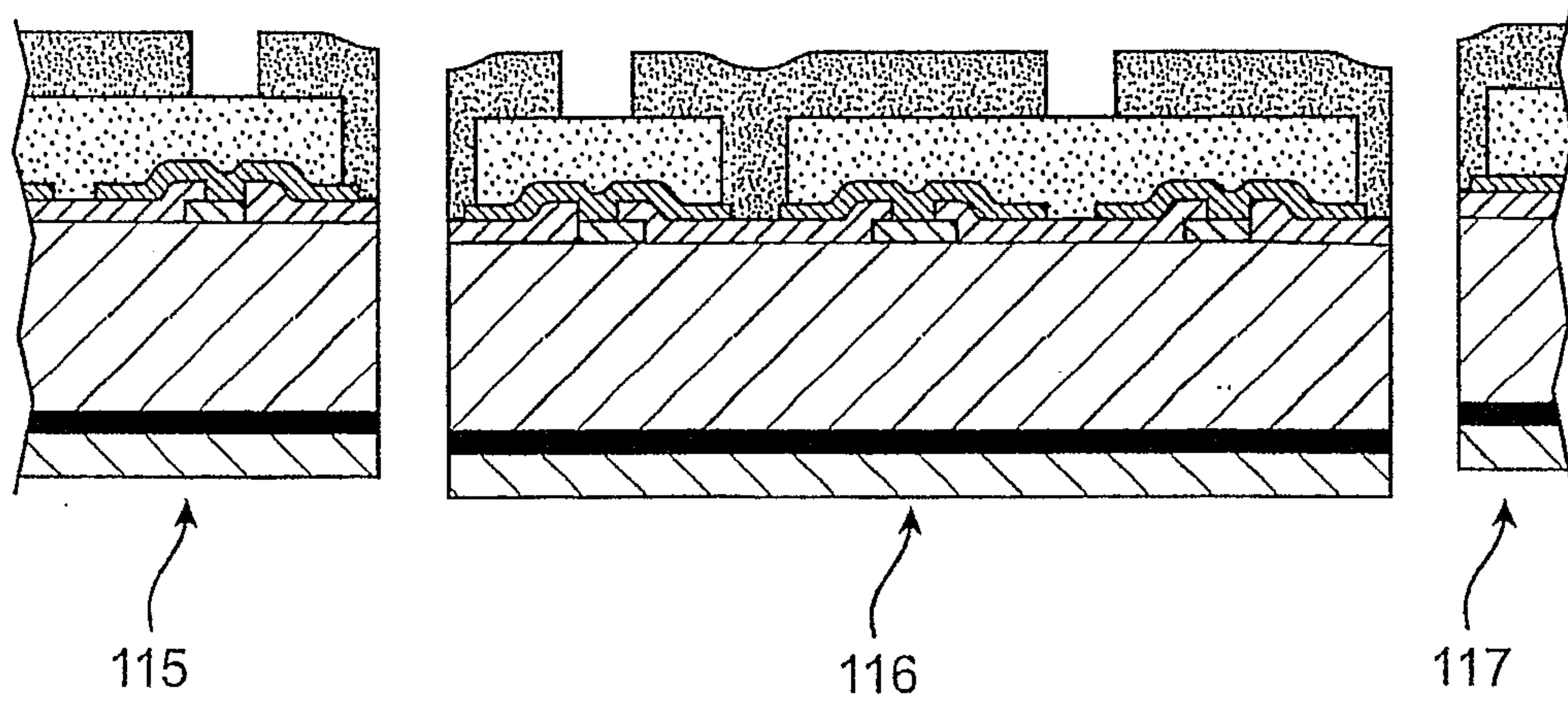


FIG. 13B

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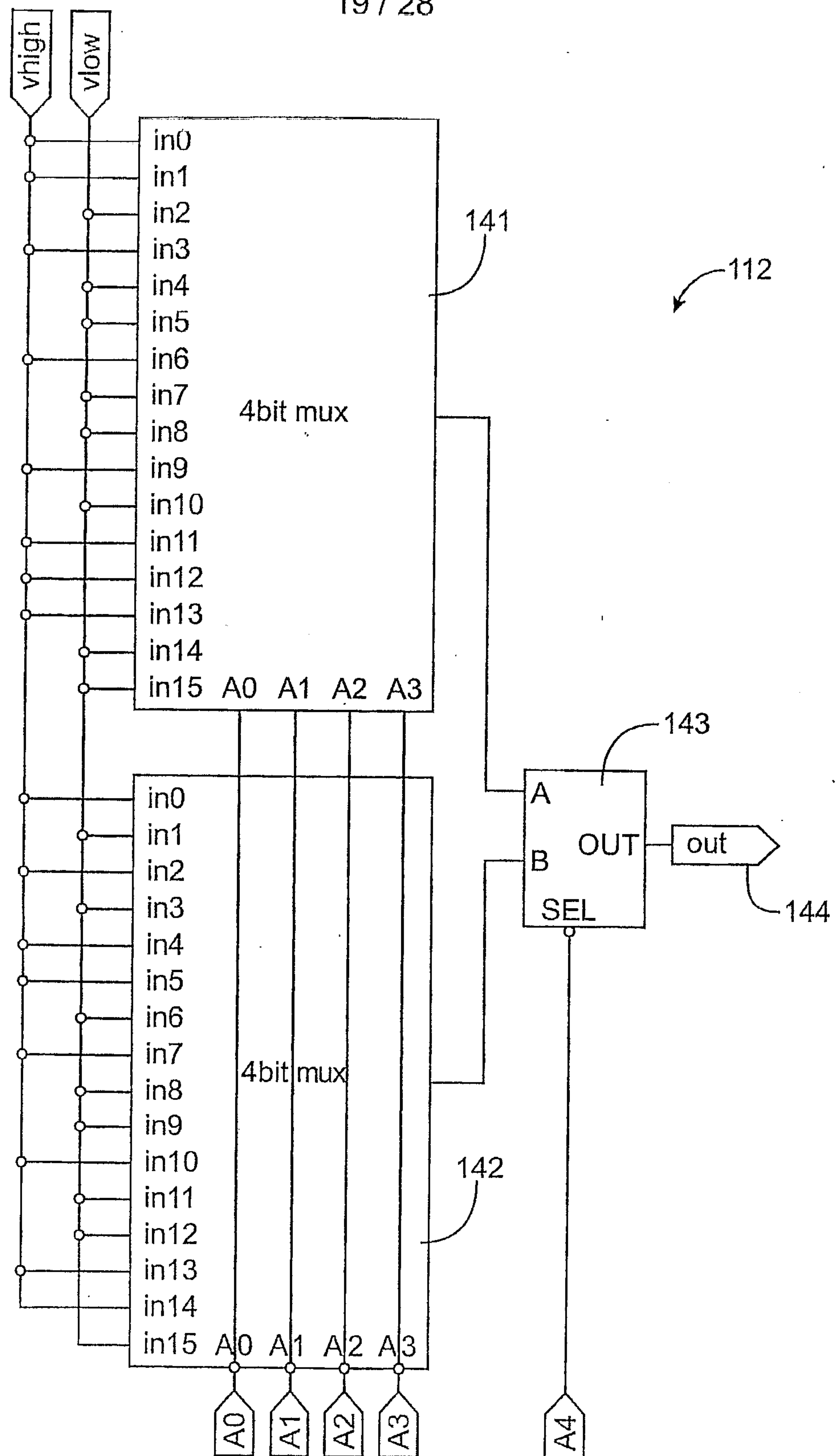


FIG. 14

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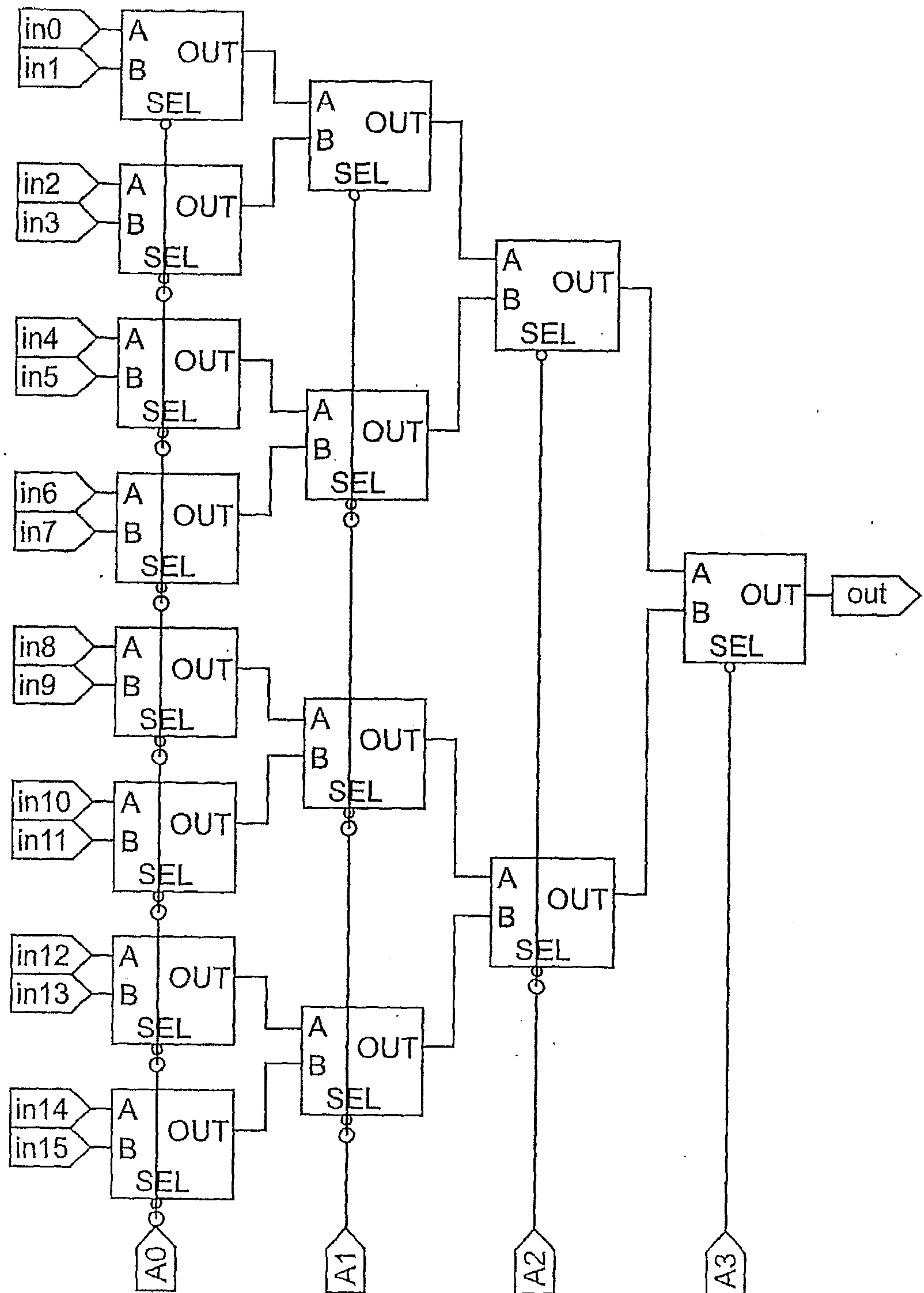


FIG. 15

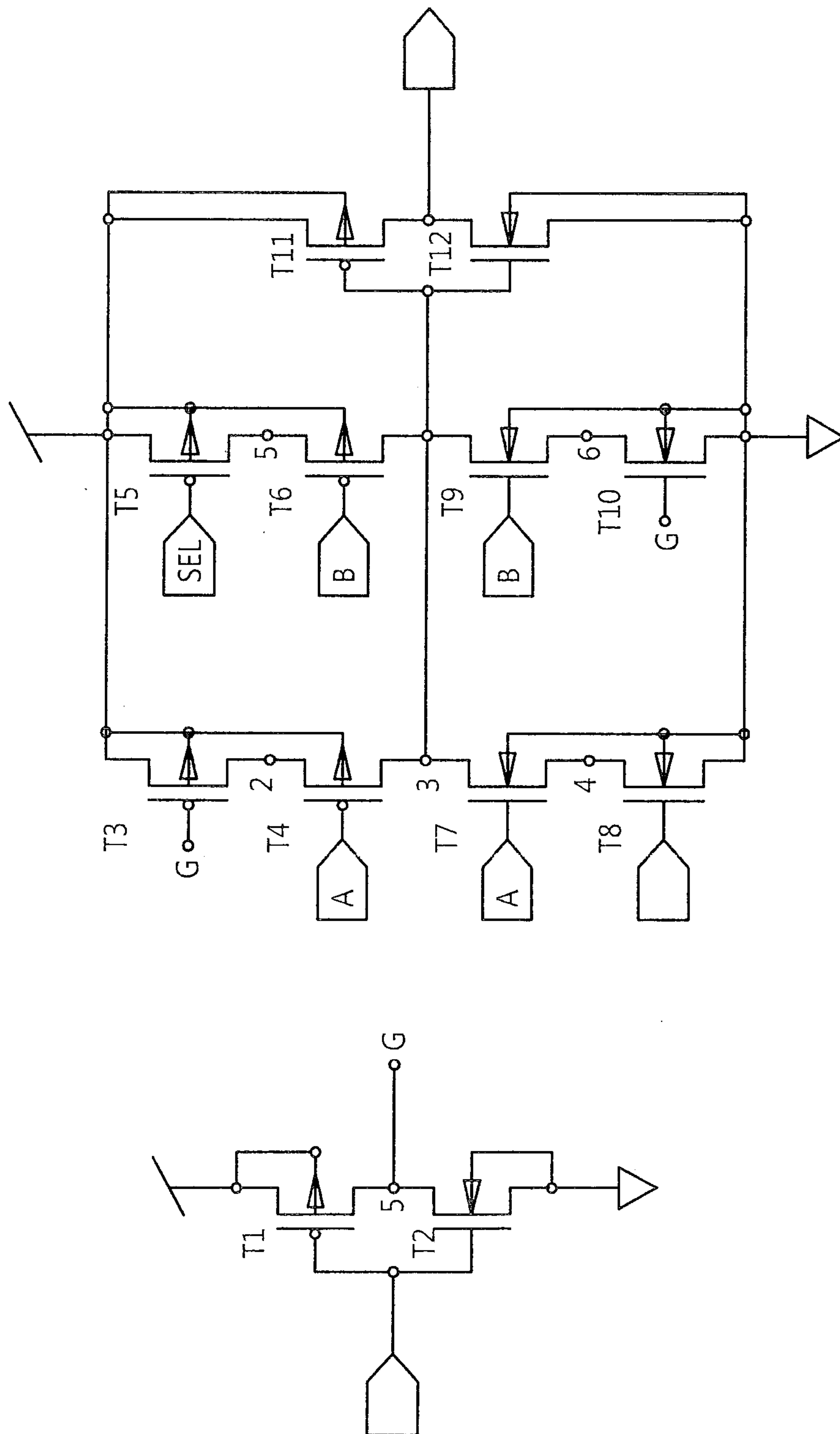


FIG. 16

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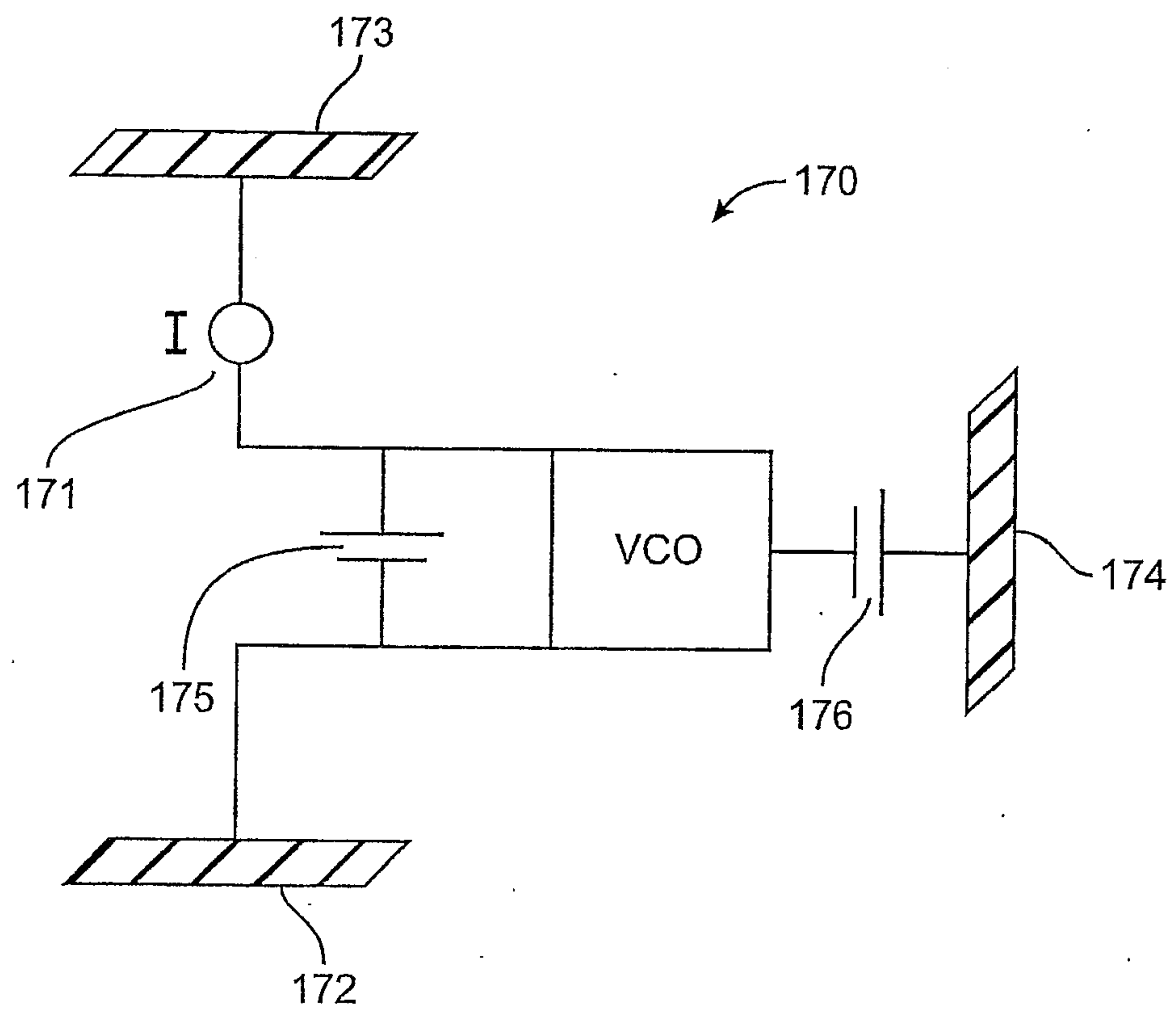


FIG. 17

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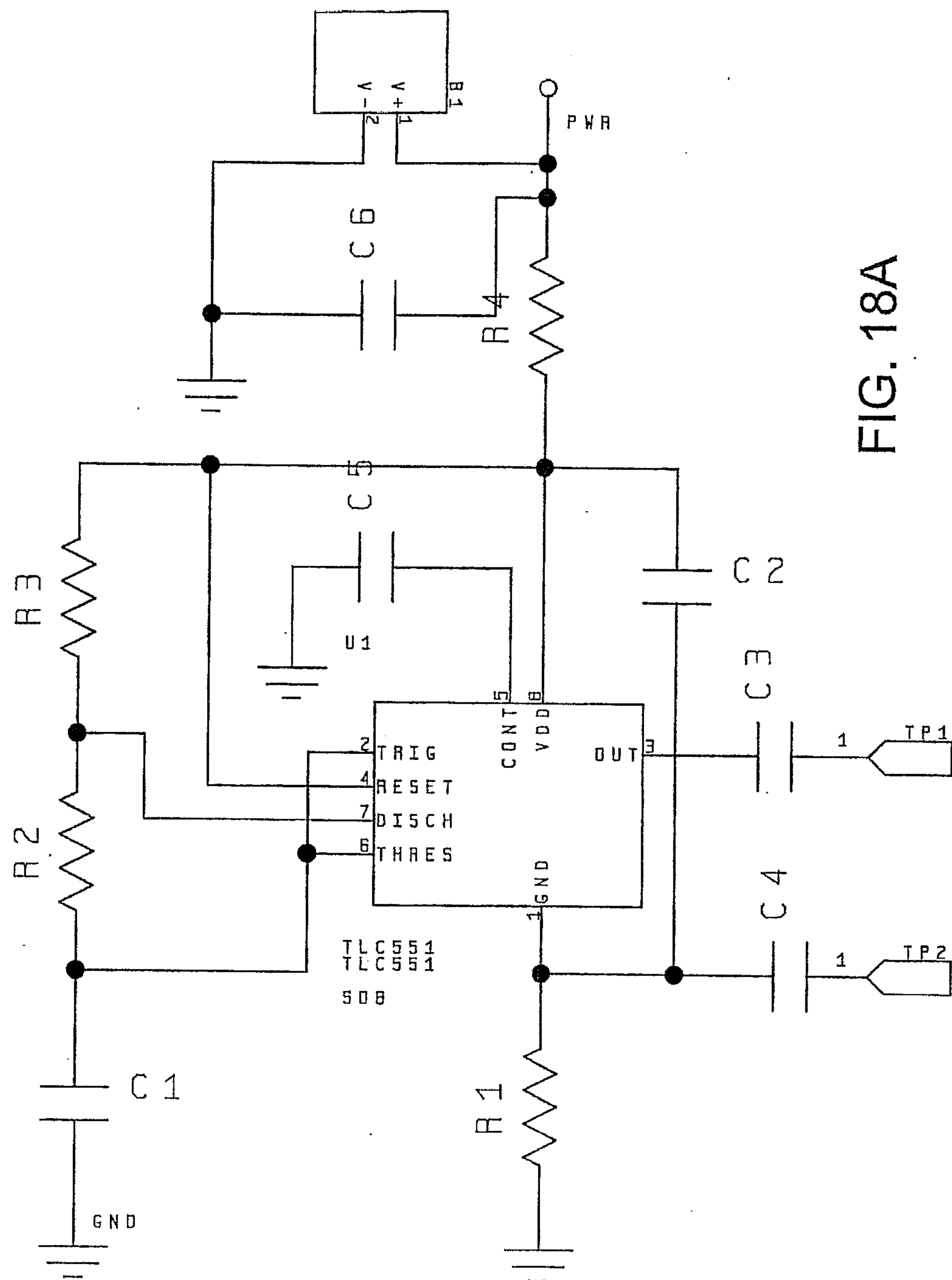


FIG. 18A

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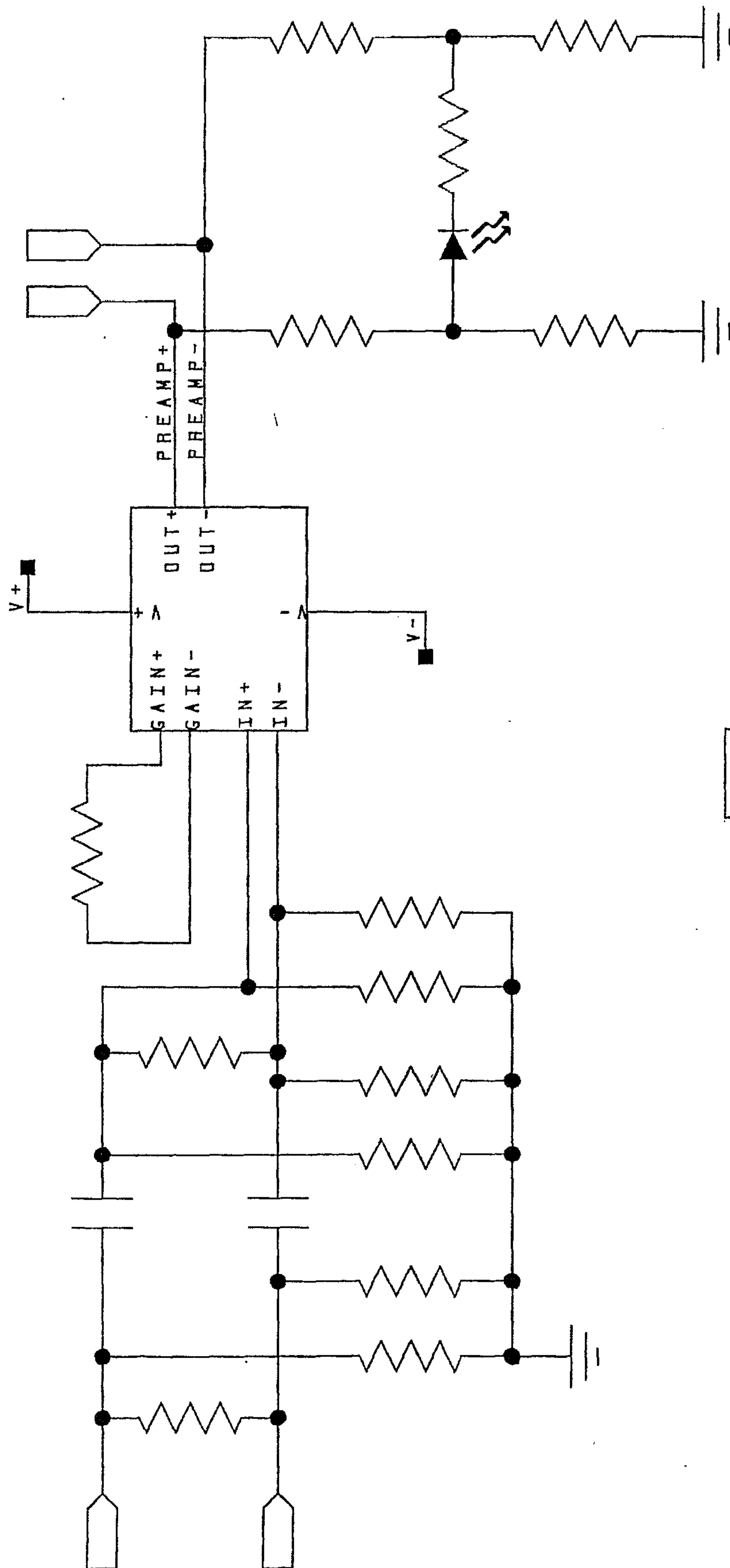
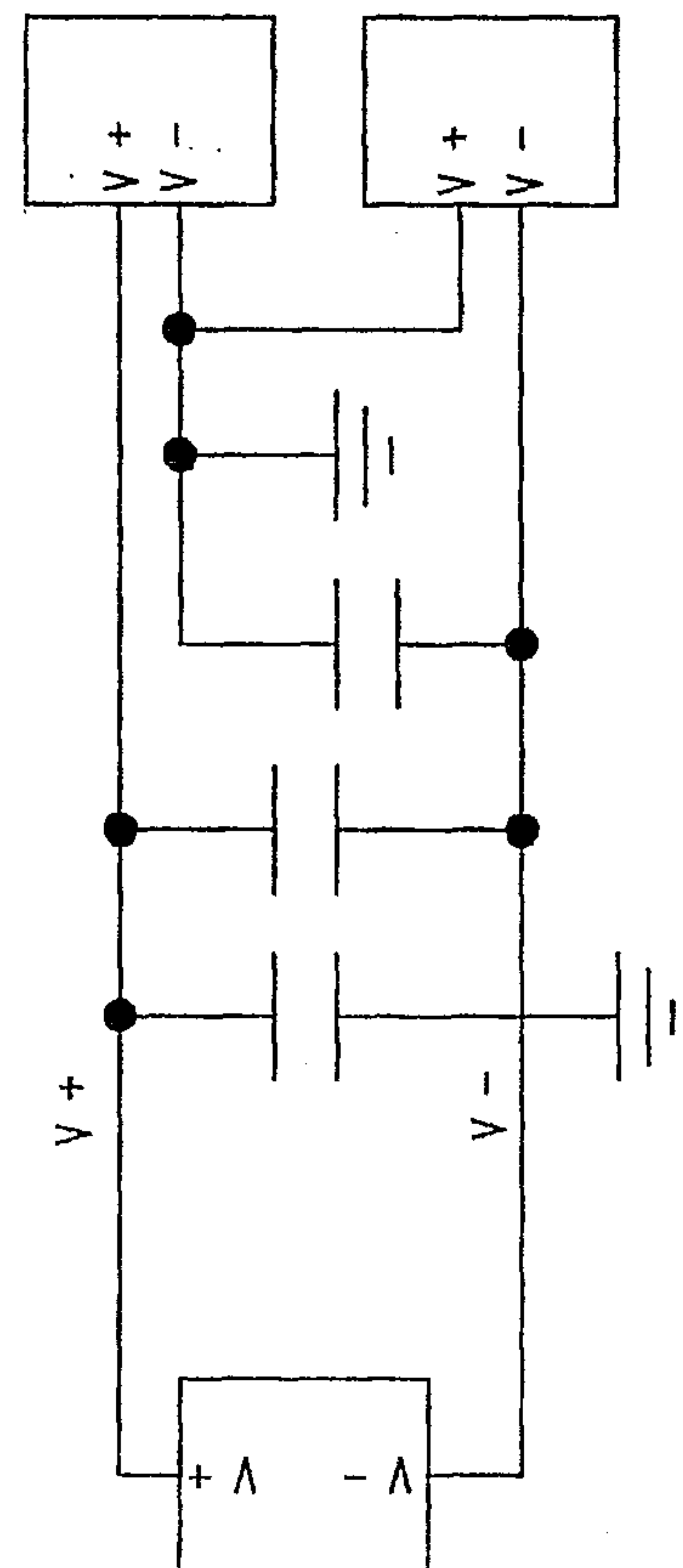


FIG. 18B1



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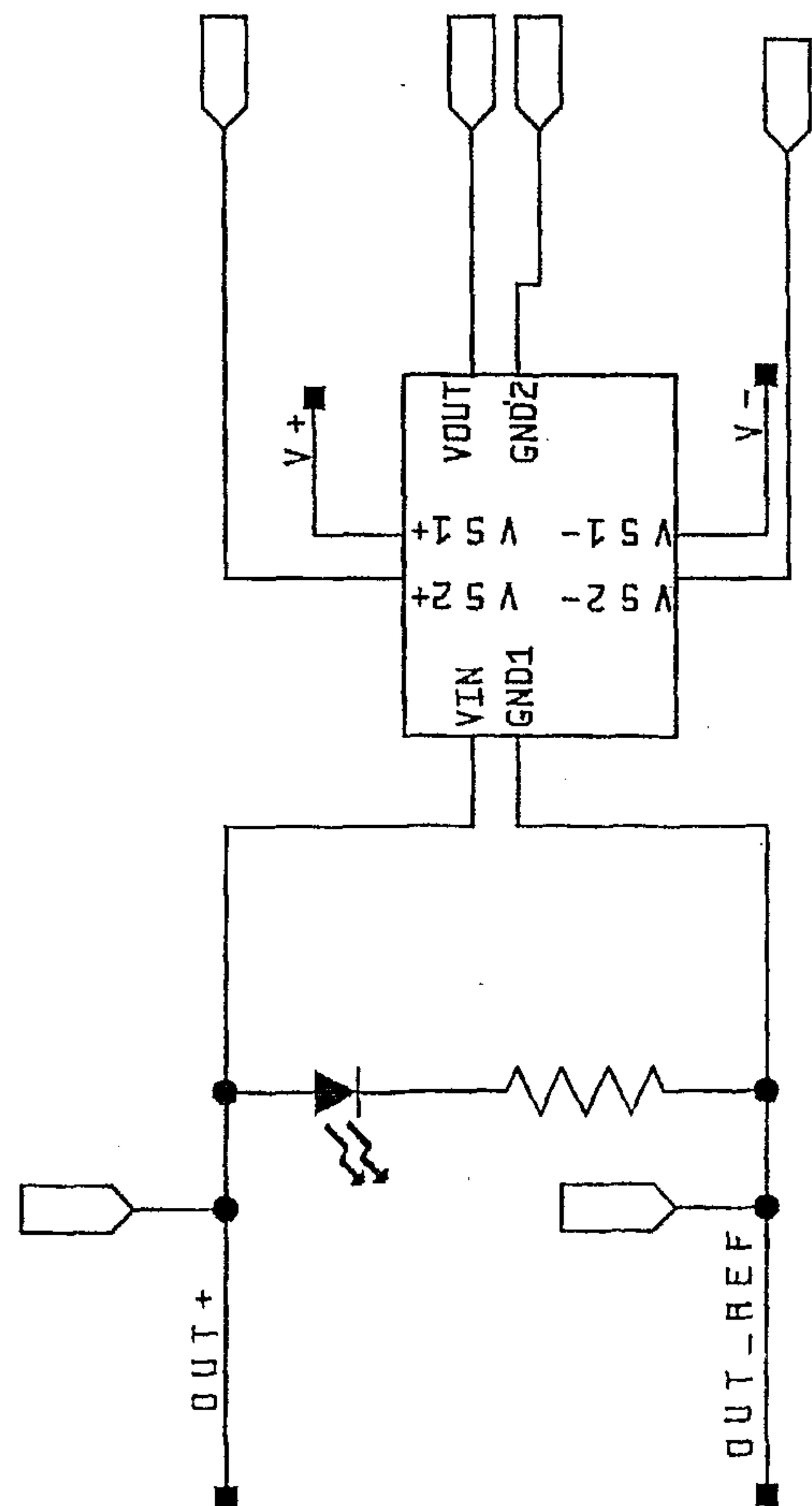
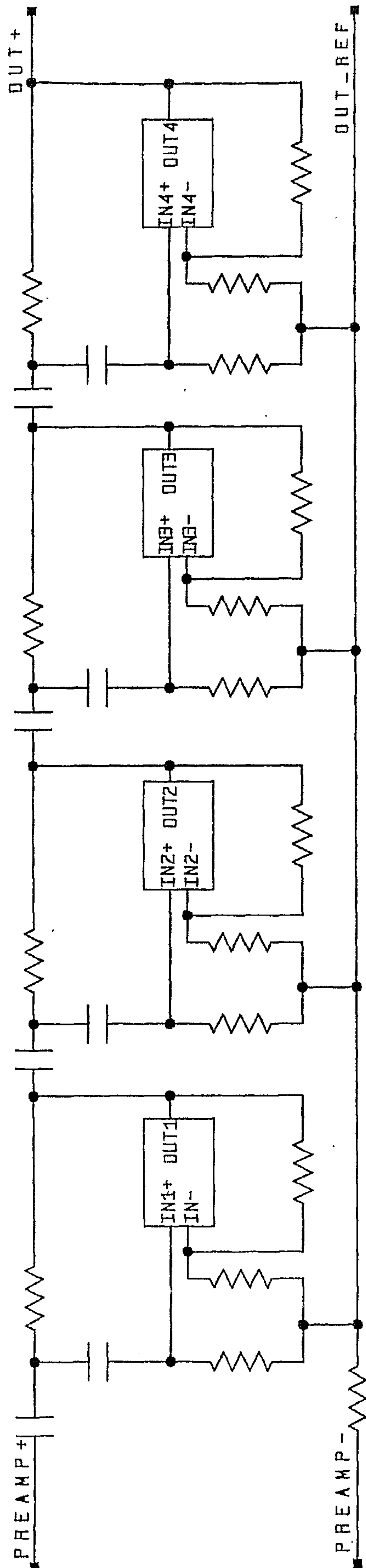


FIG. 18B2

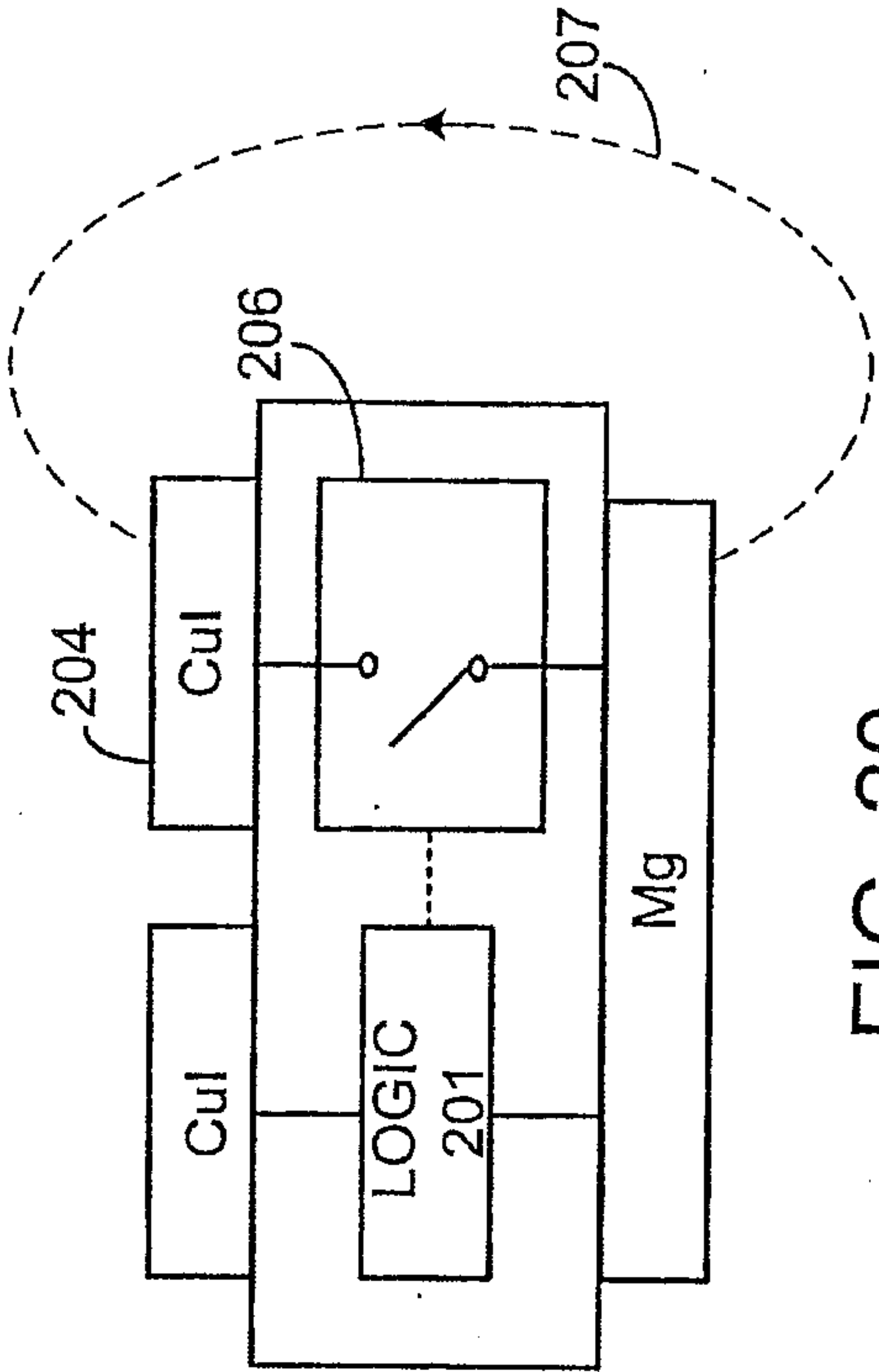


FIG. 20

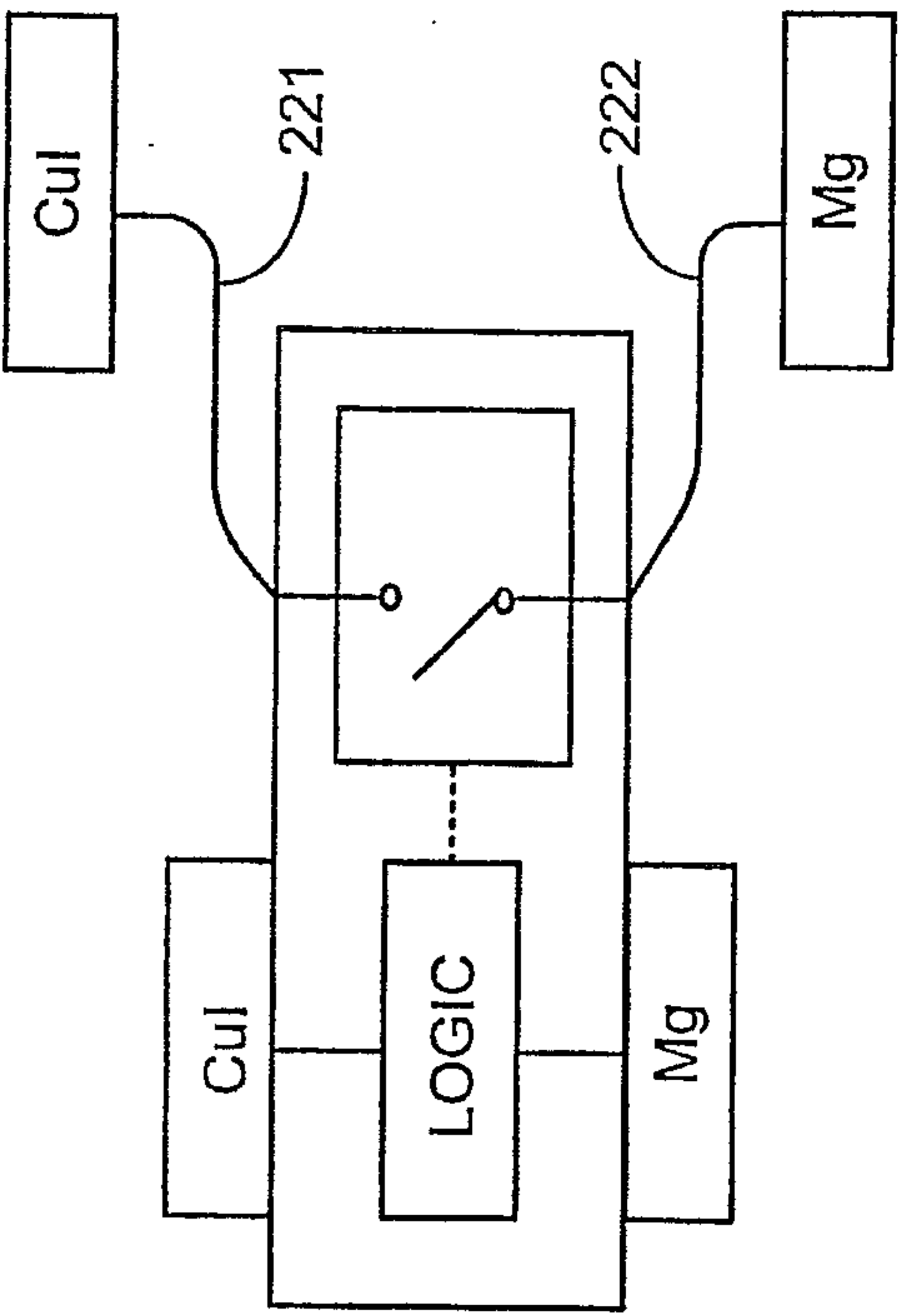


FIG. 22

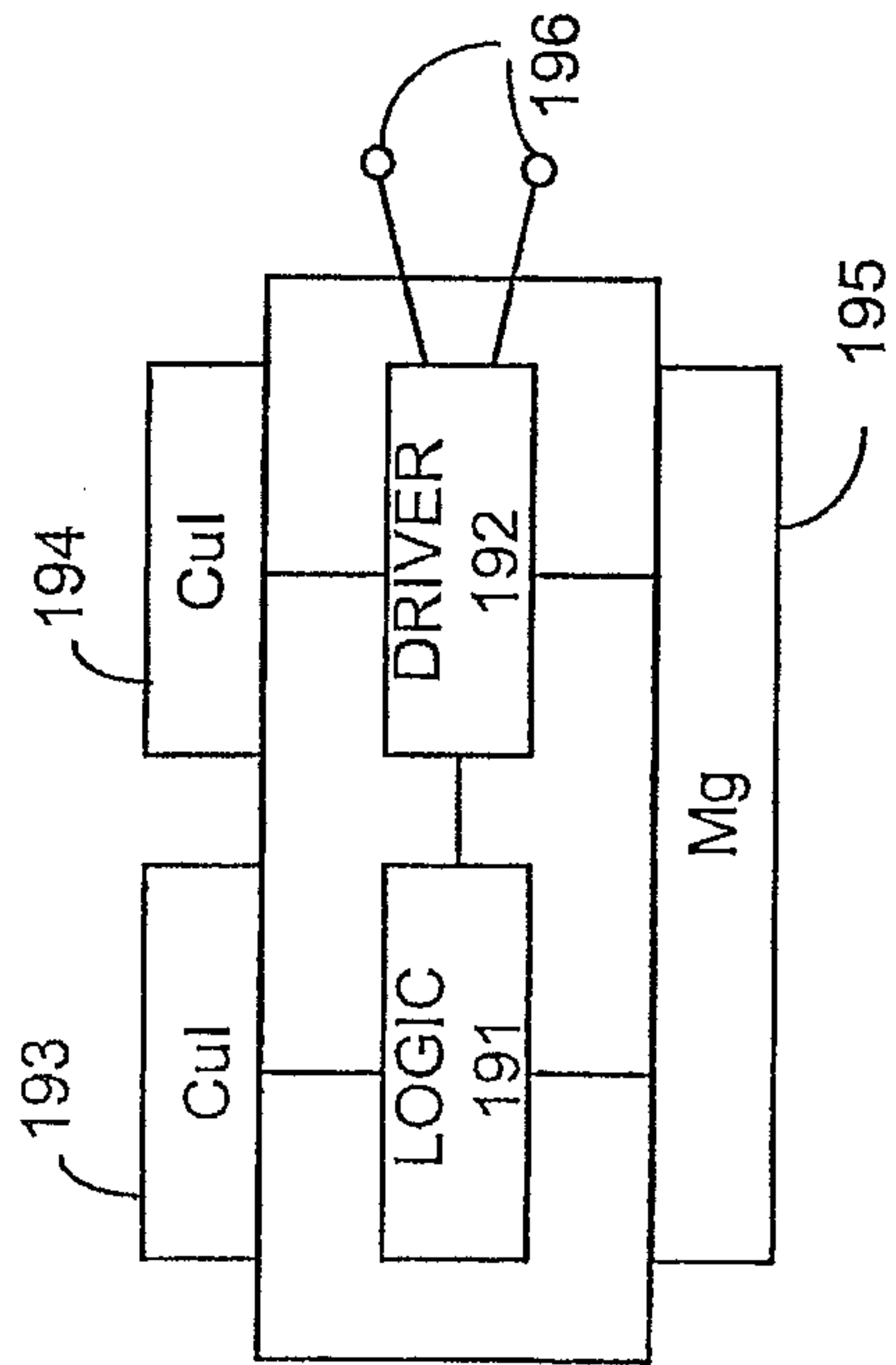


FIG. 19

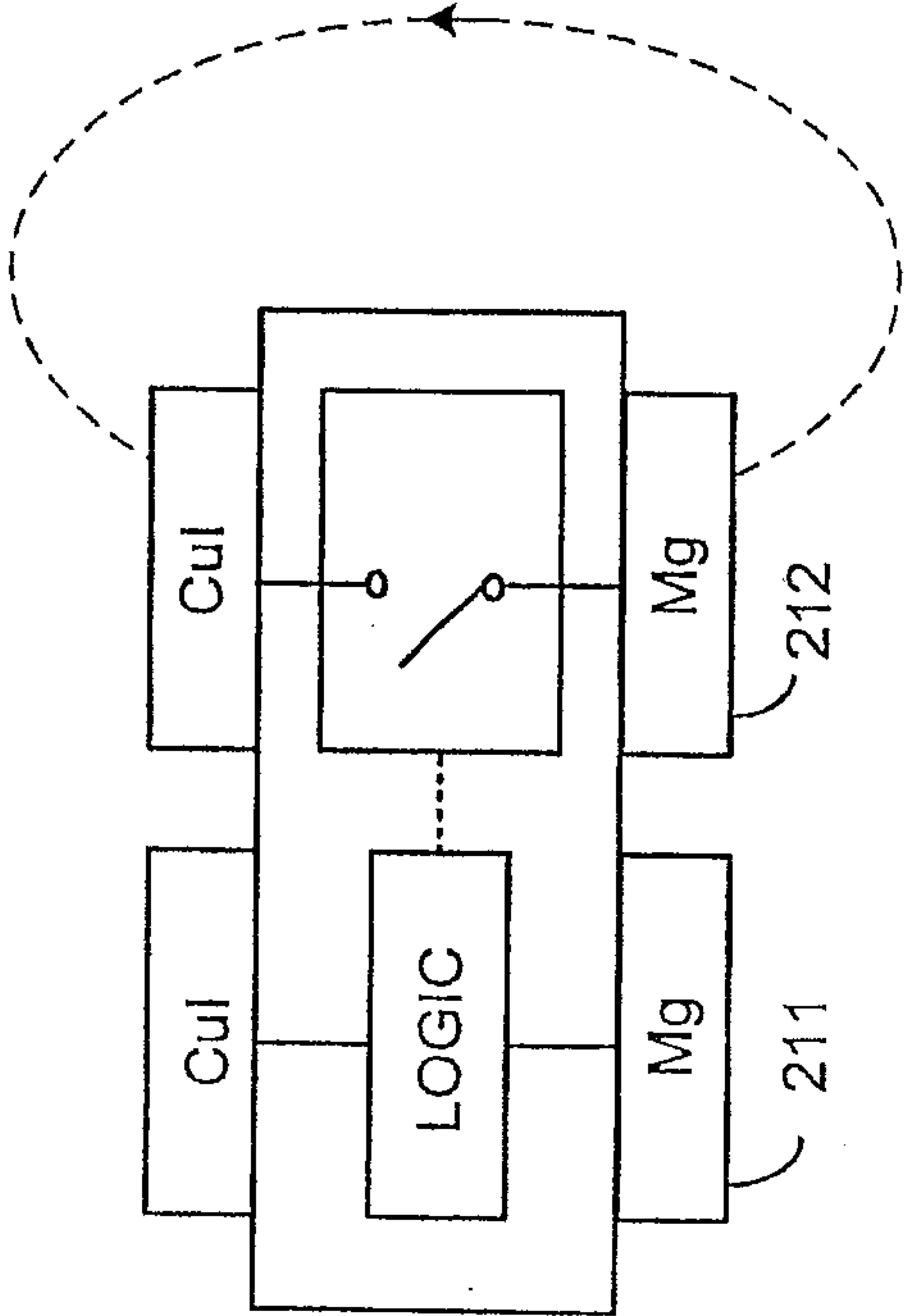


FIG. 21

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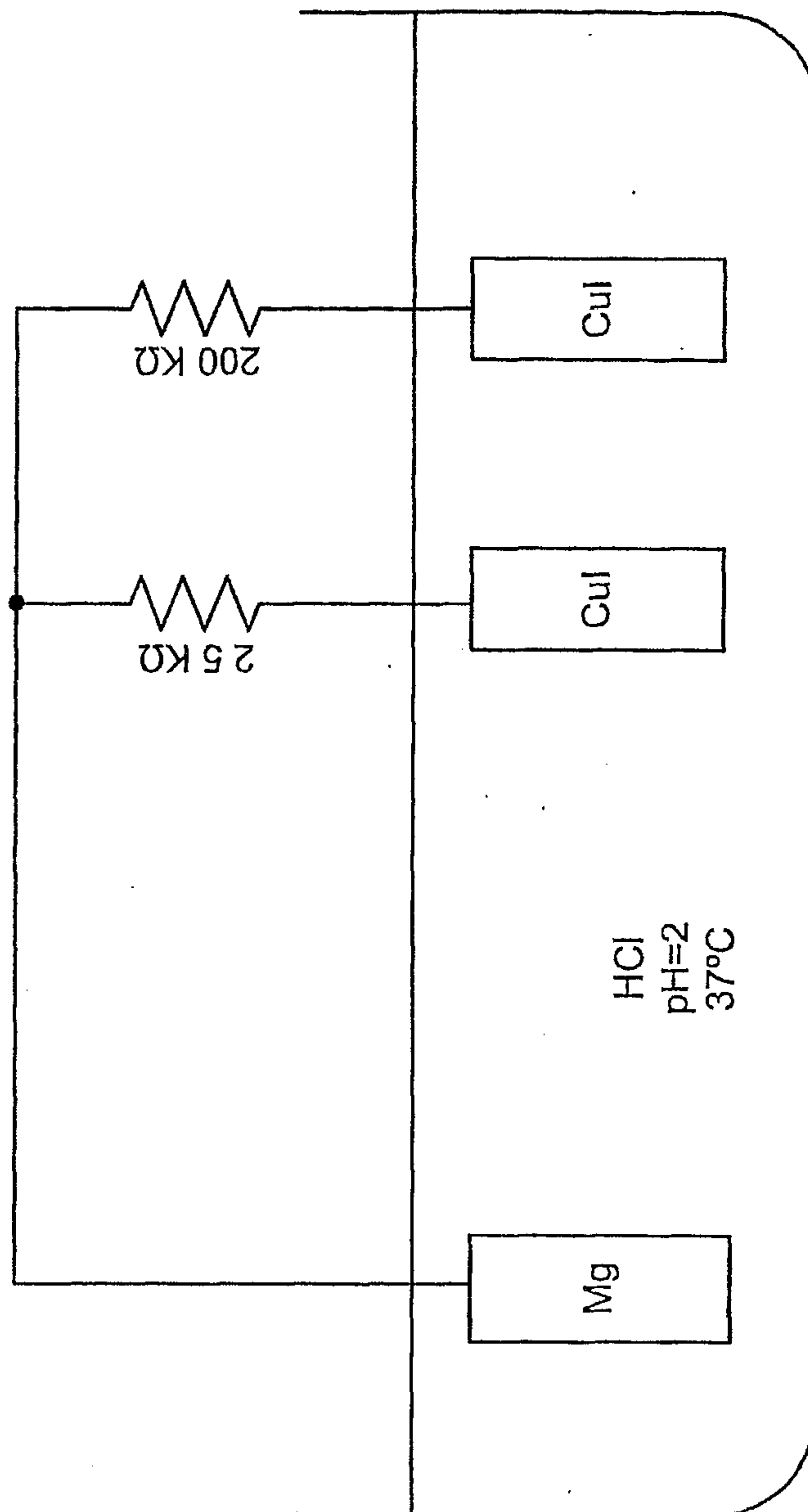


FIG. 23

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BATTERY PERFORMANCE

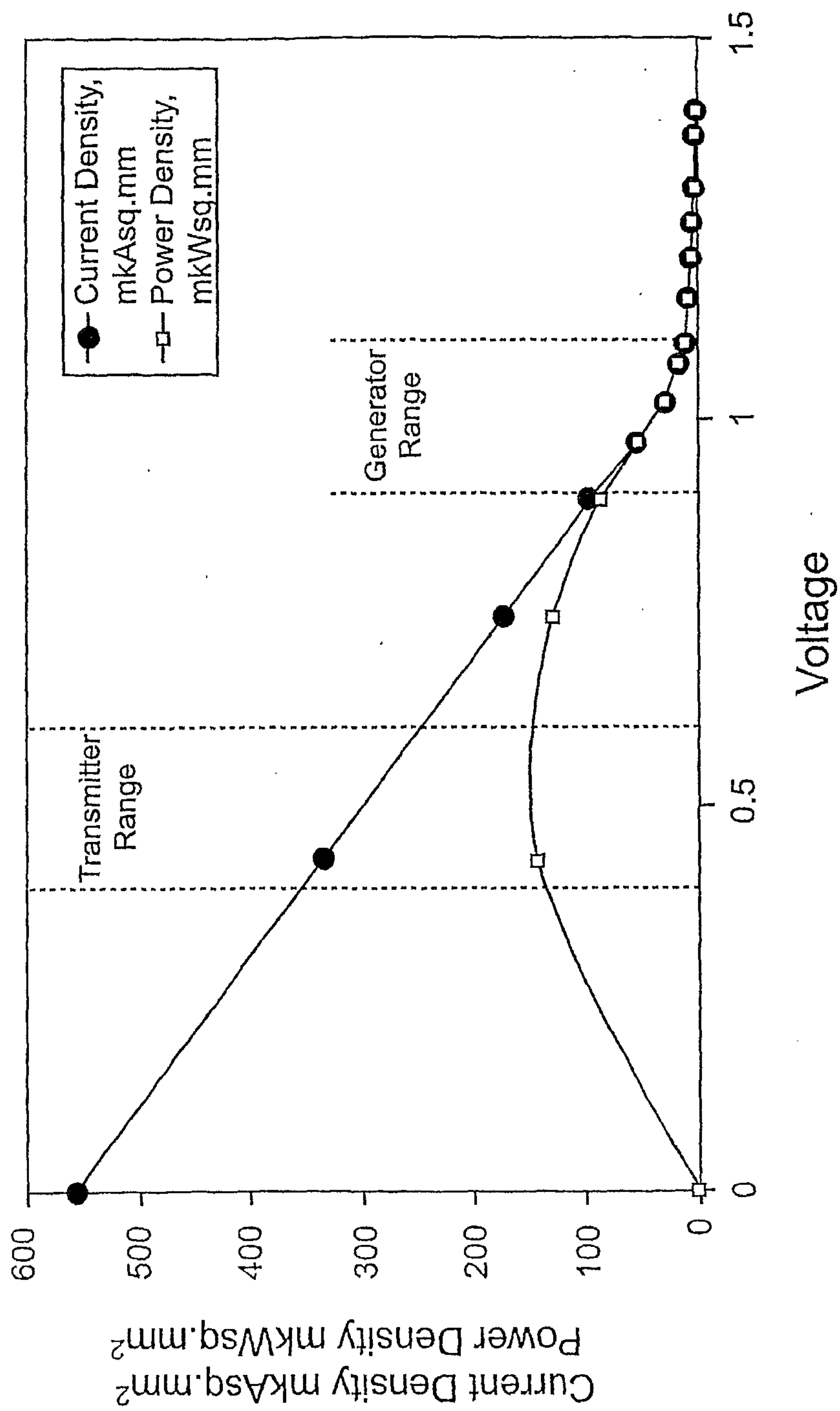


FIG. 24