



- (51) **International Patent Classification:**
A61N 2/02 (2006.01) *A61B 5/0476* (2006.01)
- (21) **International Application Number:**
PCT/US2013/035664
- (22) **International Filing Date:**
8 April 2013 (08.04.2013)
- (25) **Filing Language:** English
- (26) **Publication Language:** English
- (30) **Priority Data:**
61/621,413 6 April 2012 (06.04.2012) US
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- (81) **Designated States** (*unless otherwise indicated, for every kind of national protection available*): AE, AG, AL, AM,

AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY, BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IS, JP, KE, KG, KM, KN, KP, KR, KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

- (84) **Designated States** (*unless otherwise indicated, for every kind of regional protection available*): ARIPO (BW, GH, GM, KE, LR, LS, MW, MZ, NA, RW, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, RU, TJ, TM), European (AL, AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV, MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK, SM, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

- with international search report (Art. 21(3))
- before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments (Rule 48.2(h))

(54) **Title:** RTMS DEVICE

(57) **Abstract:** An rTMS coil or set of coils are designed to affect multiple regions of the brain with synchronous magnetic field pulses. Multiple coils aligned over the targeted regions of interest, or a single coil that is stretched or enlarged in a shape that allows the magnetic field to affect the areas of interest are disclosed. Also disclosed is a method of optimizing repetitive transcranial magnetic stimulation (rTMS) treatments.



rTMS DEVICE

CROSS-REFERENCE TO RELATED APPLICATIONS

The present application claims priority under 35 U.S.C. §119(e) to U.S. Provisional Applications No. 61/621,413, filed on April 6, 2012 the disclosure of which is incorporated herein by reference in its entirety.

FIELD OF THE INVENTION

The present invention relates to novel repetitive transcranial magnetic stimulation (rTMS) devices that are capable of stimulating two or more regions in the brain of a patient treated with such a device. The present invention also relates to graphene phased array magnets.

BACKGROUND OF THE INVENTION

Transcranial magnetic stimulation (TMS) is a procedure that uses magnetic fields to stimulate nerve cells in the brain to improve symptoms of depression and other neuropsychiatric conditions. Traditionally, TMS coils have been of a circular or figure-8 shape, designed to achieve maximum strength at a single point. For treatment of depression with standard TMS, a large electromagnetic coil is placed against or near the scalp near the forehead. The electromagnet used in TMS creates electric currents and magnetic fields that stimulate nerve cells in the region of your brain involved in mood control and depression.

The design of TMS coils can vary based on, for example, the type of material used to construct the core of the coil, the geometry of the coil configuration and the characteristics of the pulse produced by the coil. The coil is generally composed of a ferromagnetically active material and is generally called a 'solid-core' design. Several different types of coils exist, each of which produce different magnetic field patterns which include round coils, figure-eight coils, double-cone coils and four-leaf coils. Design variations in the shape of the TMS coils allows for variable penetration of the brain with the magnetic field generated by the coils. TMS devices generally are configured to treat one area of the brain at a time. In cases where multiple areas of the brain are desired to be treated then sequential treatments of the different regions of the brain are required.

The present invention provides novel rTMS devices that are capable of stimulating two or more regions in the brain of a patient treated with such a device when rTMS is required to generate synchronous TMS pulses that affect multiple regions of the brain.

SUMMARY OF THE INVENTION

Briefly, in accordance with the present invention, a repetitive transcranial magnet stimulation (rTMS) device is used to treat neuropsychiatric conditions or to improve physiological functions wherein the device contains a housing that conforms to the shape of a head of a patient or a portion of the patient's head and a coil to deliver a magnetic field. The coil configuration produces a magnetic field capable of delivering magnetic stimulation to two or more regions of a brain of a patient fitted with the rTMS device. The coil configuration comprises 2 or more coils or alternatively a single coil that is shaped to deliver magnetic stimulation to two or more regions of the brain of the patient. The geometry of the coil configuration can be a phased-array of magnetic field emitting devices, allowing complex geometries and emission fields.

Additionally, the rTMS device of the present invention can be a cap worn by a patient that has a plurality of graphene magnetic emitters that make up an array. The cap is made of any fabric such as a cloth fabric mesh. Synthetic polymer meshes can also be used. The emitters are affixed to the cap to make an array of emitters across the whole head of the patient. The cap is worn on the head of the patient where the emitters can produce desired magnetic fields by programming software that controls each emitter. The array's elements are driven by software that turns on and off each emitter to optimize the shape and placement of the magnetic lobes resulting in a phased array. The cap can additionally be fitted with touch-less EEG sensors so that a patient's EEG can be monitored in addition to providing rTMS.

The rTMS device of the present invention can deliver magnetic stimulation to the front and rear regions of the brain; the motor cortex and frontal cortex regions of the brain; or the lateral sides of the frontal lobe region of the brain. Preferably, the coil configuration is synchronized to promote coherence and synchronous behavior between multiple locations in the brain.

The present rTMS device can be used to enhance or improve physiological functions and to treat neuropsychiatric disorders or conditions. Physiological functions include concentration, sleep, alertness, memory, blood pressure, stress, libido, speech, motor function, physical performance, cognitive function, intelligence, height (in children) and

weight. A neuropsychiatric condition or disorder includes Autism Spectrum Disorder (ASD), Alzheimer's disease, ADHD, schizophrenia, anxiety, chronic pain, depression, coma, Parkinson's disease, substance abuse, bipolar disorder, a sleep disorder, an eating disorder, tinnitus, traumatic brain injury, post traumatic stress syndrome, and fibromyalgia.

Of particular interest in practicing the present invention is an rTMS device that is used to treat disorders that have poor coherence across different regions of the brain, such as, for example, Alzheimer's disease, speech and language disorders, schizophrenia and depression, by providing a device that can treat 2 or more regions of the brain simultaneously.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 shows an embodiment of a db graphene emitter.

FIG. 2 shows an embodiment of a yy graphene emitter.

FIG. 3 shows a touch-less EEG sensor.

FIG. 4 is a top view of a patient wearing a rTMS cap that contains two types of graphene emitters and touch-less EEG sensors.

FIG. 5 is a top view of a patient wearing a rTMS cap that contains two types of graphene emitters.

FIG. 6 is a top view of a patient wearing a rTMS cap that contains two types of graphene emitters.

FIG. 7 shows a multi-loop coil that provides separate magnetic field sources at various regions of the brain. The coils are connected together so as to provide a set of synchronized magnetic fields across the brain.

FIG. 8 shows a phased array configuration. In this configuration, the phase of the magnetic field pulses may be altered so as to provide additive or subtractive interference with each other, thereby creating a specific magnetic field pattern.

FIG. 9 shows the results of an EEG and brainwave map including the power distribution in a top view topography on an individual before treatment with rTMS.

FIG. 10a shows a normal figure 8 coil and FIG. 10b shows an extended or elongated figure 8 coil that produces a magnetic field that stretches along the region underneath the coil, influencing all areas of the brain that lie within this region.

DETAILED DESCRIPTION OF THE INVENTION

In practicing the present invention, a repetitive transcranial magnetic stimulation (rTMS) device is made to contain a housing that conforms to the shape of a head of a patient and/or to one or more portions of a human head. Different sizes can be made to treat pediatric, adolescent and adults. The present device also contains a coil to deliver a magnetic field. The coil configuration produces a magnetic field capable of delivering magnetic stimulation to two or more regions of a brain of a patient fitted with the rTMS device. The coil configuration can be 2 or more coils or, alternatively, a single coil that is shaped to deliver magnetic stimulation to two or more regions of the brain of the patient. Alternatively, the geometry of the coil configuration may be a phased-array of magnetic field emitting devices, allowing complex geometries and emission fields. Graphene-based magnets are also useful in the practice of the present invention.

In a preferred embodiment of the present invention, the rTMS device is a hat or a cap worn by a patient where the cap has a plurality of magnetic graphene emitters that make up an array. The cap is made of any fabric such as a cloth fabric mesh. Synthetic polymer meshes can also be used. The emitters are affixed to the cap to make an array of emitters across the whole head of the patient. The cap is worn on the head of the patient where the emitters can produce desired magnetic fields by programming software that controls each emitter. The array's elements are driven by software that turns on and off each emitter to optimize the shape and placement of the magnetic lobes resulting in a phased array. FIG. 5 shows a top view of an rTMS cap fitted on a patient where the nose 501 is seen at the top of the drawing and the ears 502, 503 are seen at the sides.

The present emitters are used to create a flat-foot-print, curved placement, coordinated phased-array using graphene emitters. Graphene (carbon nano-tube fibers) wire is used to make small coils. Because of the very low resistance that graphene has and the nano structure of the graphene fibers, very small electromagnetic coils can be made as opposed to current electromagnetic coils which require large diameter wires in order to reduce the resistance that result in bulking, heavy coils. The small size of the graphene electromagnetic coils allows for many unique applications especially when combined with sensors. Such applications include but are not limited to medical applications employing magnetic stimulation, industrial processing, biological mixing, breaking up biofilms, colloidal processing, magneto drives and the like. In such applications the graphene electromagnetic coils can be made in different spatial configurations where each configuration creates a specific magnetic field. The use of differently shaped graphene

electromagnetic coils can be used to optimize overall magnetic field direction properties desired for any given application.

One type of graphene electromagnetic coil or graphene emitter is shown in FIG. 1 which is called a dog-bone (db) emitter where the graphene fibers are coiled in a dog-bone shape. In FIG.1 an oblong central shaft 105 is covered with graphene fiber coils (emitters) 106 and is contained in winding disc 103. A magnetic radiating shell 104 covers the graphene coils 106. A cable strain relief 101 runs to a processing unit (not shown). Rim 107 contains the winding disc and is attached to a substrate 108 by threads 102. The substrate is any materials where it is desired to have the db emitter in use such as, for example, a cap in the application of an rTMS device as described herein. When electricity is passed through the db emitter the magnetic field spills out of the ends of the emitter and the lobes are wide and globular. In a TMS application this would produce skull penetration and will attract or repel other lobes from other emitters back to the brain.

Another type of graphene electromagnetic coil or graphene emitter is shown in FIG. 2 which is called a yo-yo (yy) emitter where the graphene fibers are coiled in a shape like a yo-yo string would be attached to a yo-yo. In FIG.2 a round central shaft 201 is covered with graphene fiber coils (emitters) 206 and is contained in a magnetic radiating shell 203. A cable strain relief 202 runs to a processing unit (not shown). The emitter is attached to a substrate 204 by thread 205. The substrate is any material where it is desired to have the db emitter in use such as for example a cap in the application of a TMS device as described herein. When electricity is passed through the yy emitter, the majority of the magnetic field spills out of the ends of the round shaft 201 perpendicular to the graphene fiber coils 206. In an rTMS application one half of the generated magnetic field would be directed to the skull and the other half away from the head.

The present graphene electromagnetic coils are preferably used with a sensor where the particular sensor would be chosen for the particular use of the coils. For TMS application a touch-less dry electrode EEG sensor would be used in combination with the graphene emitters. Touch-less dry electrode EEG sensors are commercially available from Cognionics, San Diego, CA. FIG. 3 shows an EEG touch-less dry-electrode EEG sensor that contains a PCB board 303 housed in an EEG sensor shell 301. A cable strain relief 302 runs to a processing unit (not shown). The sensor is attached to a substrate 305 by thread 304.

In a preferred embodiment of the present invention, db emitters, yy emitters and touch-less dry electrode EEG sensors are used to make a TMS cap that can both detect EEG

patterns and administer transcranial magnetic stimulation to a patient by producing a phased array effect.

As shown in FIG. 4, each emitter 404, 405 and EEG sensor 406 is a generally flat disc 404, 405 and 406 that is in the basic shape of a circle. The emitters and sensors are butted-up against each other, attached to the fabric mesh, and vary in starting sequence and vary in position from row to row. The emitters 404, 405 and sensors 406 are connected by wires (not shown) to a control panel (not shown) that contains the programmed software and power supply. There are two types of emitters shown in FIG. 4 and are named herein based on their shape. One is referred to as the dog-bone (db) emitter 404 and the other is referred to as the yo-yo (yy) emitter (405). There are two preferred patterns for placing the emitters and sensors on the cap: (1) -[db]-[eeg]-[yy]- and (2) -[yy]-[eeg]-[db]-. The basic pattern that is laid-down and attached is follows:

-[db]-[eeg]-[yy]-[db]-[eeg]-[yy]-[db]-[eeg]-[yy]-
 -[db]-[yy]-[eeg]-[db]-[yy]-[eeg]-[db]-[yy]-[eeg]-
 -[eeg]-[yy]-[db]-[eeg]-[yy]-[db]-[eeg]-[yy]-[db]-
 -[db]-[eeg]-[yy]-[db]-[eeg]-[yy]-[db]-[eeg]-[yy]-
 -[db]-[yy]-[eeg]-[db]-[yy]-[eeg]-[db]-[yy]-[eeg]-
 -[eeg]-[yy]-[db]-[eeg]-[yy]-[db]-[eeg]-[yy]-[db]-

The emitters 404, 405 and sensors 406 are sewn on, or attached by other means, like buttons, over the whole cloth mesh fitted to cover a head. The sensors and emitters should not overlap. An average size cap will contain 45 eeg sensors, 45 Db emitters, and 45 Yy emitters.

The two types of emitters, db and yy, produce an array that is used to shape and optimize the magnetic field direction. This "Phased-Array" is controlled by software and the magnetic field can be adjusted accordingly. The phasing of the magnetic array is accomplished through software control of the magnitude, position and orientation of each separate emitter, in sequence, through time. Since opposite fields attract each other, the lobes can effectively be focused to a targeted area of the scalp and underlying brain structures. The size of the emitters and sensors is not critical to the practice of the present invention. The diameter of the emitters and sensors is typically in the range of 15– 30 millimeters (mm) and preferably 17-19mm. An average size cap will contain about 45 eeg sensors, 45 db emitter and 45 yy emitters.

In the yy emitters the majority of the magnetic field spills out the ends of the post, perpendicular to the direction of the disks. So half of the field tends toward the direction of the brain, as the yy emitter lays on its side, against the head and the other half out into space away from the brain. In the db emitters the opposite happens. The magnetic field spills out the ends of the db emitter tending toward parallel to the side of the skull where the lobes still are fairly wide, and globular providing skull penetration. More importantly the db emitters are better in attracting, or repelling, other lobes back towards the brain, and determining the direction of lobes in the phased-array.

The focusing of these arrays of magnetic lobes is useful in the practice of the present invention. As an example a cluster of 3-7 of the yy emitters will drive the primary magnetic lobes on one side of the head. The db emitters on the same side will help shape and stretch these primary lobes. The yy and db emitters on the other side of the head will shape and stretch the lobes to the preferred target areas in greatest concentration, hence phased-arrays.

FIG. 5 shows is a top view of a patient wearing a TMS cap of the present invention that contains db emitters 504 and yy emitters 505 but no EEG sensors. Orientation of the cap is seen by the patient's nose 501 and ears 502, 503. The emitters 504, 505 are generally flat discs that are in the basic shape of a circle. The emitters are butted-up against one another, attached to the fabric mesh substrate, and vary in starting sequence and vary in position from row to row. The emitters 504, 505 are connected by wires (not shown) to a control panel (not shown) that contains the programmed software and power supply. Preferably, the emitters are arranged in an alternating configuration as depicted in FIG. 5. The emitters 504, 505 are sewn on, or attached by other means, like buttons, over the whole cloth mesh fitted to cover a head and should not overlap. An average size cap will contain about 125 or more emitters. This TMS cap is used to administer repetitive TMS to a targeted area of the brain.

FIG. 6 is another top view of a patient wearing a TMS cap of the present invention that contains db emitters 604 and yy emitters 605 but no EEG sensors. Orientation of the cap is seen by the patient's nose 601 and ears 602, 603. The emitters 604, 605 are generally flat discs that are in the basic shape of a circle. The emitters are butted-up against one another, attached to the fabric mesh substrate, and vary in starting sequence and vary in position from row to row. The emitters 504, 505 are connected by wires (not shown) to a control panel (not shown) that contains the programmed software and power supply. The embodiment shown in FIG. 6 is similar to the embodiment shown in FIG.5 with the exception that less emitters are employed.

The focusing of these arrays of magnetic lobes is useful in the practice of the present invention. As an example a cluster of 3-7 of the yy emitters will drive the primary magnetic lobes on one side of the head. The db emitters on the same side will help shape and stretch these primary lobes. The yy and db emitters on the other side of the head will shape and stretch the lobes to the preferred target areas in greatest concentration, hence phased-arrays.

The rTMS device of the present invention can deliver, for example, magnetic stimulation to the front and rear regions of the brain; the motor cortex and frontal cortex regions of the brain; or the lateral sides of the frontal lobe region of the brain. Preferably, the coil configuration is synchronized to promote coherence and synchronous behavior, such as EEG wave patterns, between multiple locations in the brain.

The present rTMS device can be used to enhance or improve physiological functions and to treat neuropsychiatric disorders or conditions. Physiological functions include concentration, sleep, alertness, memory, blood pressure, stress, libido, speech, motor function, physical performance, cognitive function, intelligence, height (in children) and weight. A neuropsychiatric condition or disorder includes Autism Spectrum Disorder (ASD), Alzheimer's disease, ADHD, schizophrenia, anxiety, depression, coma, Parkinson's disease, substance abuse, bipolar disorder, a sleep disorder, an eating disorder, tinnitus, traumatic brain injury, post traumatic stress syndrome, and fibromyalgia.

Of particular interest in practicing the present invention is an rTMS device that is used to treat disorders that have poor coherence across different regions of the brain, such as, for example, Alzheimer's disease, speech and language disorders, schizophrenia and depression, by providing a device that can treat 2 or more regions of the brain simultaneously.

In one embodiment of the present invention an rTMS device is configured to treat an Alzheimer's patient by providing magnetic field stimulation to the front and rear portions of the brain. The patient is treated daily for 30 minutes with 6 seconds of magnetic stimulation per minute.

In another embodiment of the present invention an rTMS device is configured to treat a patient having a speech disorder by providing magnetic field stimulation to the motor cortex and the frontal cortex regions of the brain. The patient is treated daily for 30 minutes with 6 seconds of magnetic stimulation per minute.

In a further embodiment of the present invention an rTMS device is configured to treat a schizophrenic patient by providing magnetic field stimulation to the lateral sides of the frontal lobe of the brain. The patient is treated daily for 30 minutes with 6 seconds of magnetic stimulation per minute.

In another embodiment of the present invention an rTMS device is configured to treat a depressed patient by providing magnetic field stimulation to the lateral sides of the frontal lobe of the brain. The patient is treated daily for 30 minutes with 6 seconds of magnetic stimulation per minute.

There are several examples of disorders that result in EEG activity being incoherent or asynchronous between different brain regions. In Alzheimer's, activity between the front and rear portions of the brain tend to lack coherence. In speech and language disorders, the motor cortex is often asynchronous with the frontal cortex. In other disorders such as Schizophrenia or depression, there is often seen a lack of coherence between the lateral sides of the frontal lobe.

The symptoms of the disorder are reduced and improvement in cognitive function is achieved by administering the present rTMS pulses to entrain the regions to act in concert and synchronously.

The pulses generated by the present rTMS device to different regions of the brain are preferably synchronized together to promote coherence across the brain. The coils are oriented ergonomically with a tilt designed to fit the scalp. The rTMS device can contain multiple coils oriented to treat different regions of the brain or a single coil could be stretched so that the focus of the magnetic field is spread out in a line over a wider area. One example would be to stretch the coil so that it covers both lateral sides of the prefrontal lobe. If desired, the coil could be made larger which will cause the magnetic field to be more dispersed.

FIG. 10b shows an elongated coil that spreads the magnetic field underneath the coil to cover an area underneath the coil when used to administer rTMS to a patient. FIG. 10a is a traditional coil that does not cover the same area as the elongated coil. The coil shown in FIG. 10b can treat more than one area of the brain.

FIG. 7 shows multiple coils connected together, situated to stimulate separate regions of the brain simultaneously.

FIG. 8 shows a phased array of coils 801, intended to use phase differences in pulses to direct and target multiple regions of the brain. The coils are operated by a central processor 802 that can adjust the magnetic field produced by each coil. An on/off switch 803 is used to turn off a particular coil if desired.

An additional aspect of the present invention is a method of optimizing repetitive transcranial magnetic stimulation (rTMS) of a patient by recording the patient's whole head EEG; mapping the energy of the EEG at one or more frequencies to identify regions of

incoherent or non-synchronous brain activity; and administering rTMS to the regions of the brain that are incoherent and non-synchronous. Such an optimized process can include an rTMS device that has (a) 2 or more coils, (b) a single coil configured in such a way to deliver stimulation to 2 distinct regions of the brain, or (c) a phased-array magnetic field emitting device capable of forming complex geometries and emission fields wherein the phased array modalities are leveraged to induce positional and temporal intensities. A preferred phased array is the rTMS cap described herein. With EEG mapping, areas of low energy are identified by measuring the energy of the EEG at the interested frequency across the brain employing well known algorithm selected from the group consisting of least squares, LORETA, and focal optimization. Areas of low energy can also be identified by measuring the Q-factor (width of the frequency plot) at the one or more frequencies used to map the energy of the EEG.

FIG. 9 shows the results of an EEG and brainwave map including the power distribution in a top view topography on an individual before treatment with rTMS. The left panel shows the signals in time domain and the middle panel the frequency domain following Fast Fourier Transformation (FFT) where the dominant frequency is at 9.71 Hz. It can be seen that the dominant frequency of 9.71 is missing in some frontal channels. The right side map displays the power distribution in a top-view topography. The treatment is to convert the intrinsic frequency to a train of TTL pulses in a computer script file to trigger the TMS pulse discharge. The stimulation area will be the bilateral frontal lobe at a frequency of 9.71. The rTMS treatments started on a daily basis for 30 minutes will pull up the 9.71 Hz in those missing channels by providing stimulation at an harmonic of one of the biological signals.

The present invention may be embodied in other specific forms without departing from its spirit or essential characteristics. The described embodiments are to be considered in all respects only as illustrative and not restrictive. The scope of the invention is, therefore, indicated by the appended claims rather than by the foregoing description. All changes which come within the meaning and range of equivalency of the claims are to be embraced within their scope.

IN THE CLAIMS

We claim:

1. A repetitive transcranial magnet stimulation (rTMS) device to treat neuropsychiatric conditions or to improve physiological functions which comprises:
 - a. a housing that conforms to the shape of a head of a patient; and
 - b. a coil configuration that produces a magnetic field capable of delivering magnetic stimulation to two or more regions of a brain of a patient fitted with the rTMS device.
2. The rTMS device of claim 1 wherein the coil configuration comprises 2 or more coils.
3. The rTMS device of claim 1 wherein the coil configuration comprises a single coil that is shaped to deliver magnetic stimulation to two or more regions of the brain of the patient.
4. The rTMS device of claim 1 wherein the geometry of the coil configuration is a phased-array of magnetic field emitting devices, allowing complex geometries and emission fields.
5. The rTMS device of claim 1 wherein the device delivers magnetic stimulation to the front and rear regions of the brain.
6. The rTMS device of claim 1 wherein the device delivers magnetic stimulation to the motor cortex and frontal cortex regions of the brain.
7. The rTMS device of claim 1 wherein the device delivers magnetic stimulation to the lateral sides of the frontal lobe region of the brain.
8. The rTMS device of claim 1 wherein the pulses generated by the coil configuration is synchronized to promote coherence and synchronous behavior between multiple locations in the brain.
9. A method of optimizing repetitive transcranial magnetic stimulation (rTMS) of a patient with an rTMS device which comprises:
 - a. recording the patient's whole head EEG;

b. mapping the energy of the EEG at one or more frequencies to identify regions of incoherent or non-synchronous brain activity; and

c. administering rTMS to the regions of the brain that are incoherent and non-synchronous.

10. The method of claim 9 wherein the rTMS device comprises:

a. 2 or more coils,

b. a single coil configured in such a way to deliver stimulation to 2 distinct regions of the brain,

c. a phased-array magnetic field emitting device capable of forming complex geometries and emission fields, wherein the phased array modalities are leveraged to induce positional and temporal intensities or

d. a grapheme based magnet.

11. The method of claim 9 wherein areas of low energy are found by measuring the energy of the EEG at the interested frequency across the brain employing an algorithm selected from the group consisting of least squares, LORETA, and focal optimization.

12. The method of claim 9 wherein areas of low energy are found by measuring the Q-factor (width of the frequency plot) at the one or more frequencies used to map the energy of the EEG.

13. A TMS cap which comprises:

a. a cap base that fits over the head of a patient;

b. a plurality of graphene magnetic emitters having a first configuration;

c. a plurality of graphene magnetic emitters having a second configuration

wherein the placement of the graphene emitters produces a phase array effect when the emitters are activated.

14. The TMS cap of claim 13 wherein the first configuration is a db emitter configuration and the second configuration is a yy emitter configuration.

15. The TMS cap of claim 14 further comprising:

d. a plurality of touch-less EEG sensors.

16. A repetitive transcranial magnet stimulation (rTMS) device to treat neuropsychiatric conditions or to improve physiological functions which comprises a plurality of graphene magnetic emitters in a configuration that produces a magnetic field capable of delivering magnetic stimulation to two or more regions of a brain of a patient fitted with the rTMS device.

17. The rTMS device of claim 16 wherein the geometry of the graphene magnetic emitters is a phased-array of magnetic field emitting devices, allowing complex geometries and emission fields.

18. The rTMS device of claim 17 wherein the graphene magnetic emitters comprise db emitters and yy emitters

19. A TMS cap which comprises:

- a. a cap base that fits over the head of a patient;
- b. a plurality of graphene magnetic emitters having a first configuration;
- c. a plurality of graphene magnetic emitters having a second configuration; and
- d. a plurality of touch-less EEG sensors

wherein the placement of the graphene emitters produces a phase array effect when the emitters are activated and the touch-less EEG sensors measure brain wave patterns when the sensors are activated.

20. The TMS cap of claim 19 wherein the first configuration is a db emitter configuration and the second configuration is a yy emitter configuration.

21. A TMS cap which comprises:

- a. a cap base that fits over the head of a patient;
- b. a plurality of graphene magnetic emitters having a first configuration;
- c. a plurality of graphene magnetic emitters having a second configuration;
- d. a plurality of touch-less EEG sensors;
- e. a wire attached to each emitter and sensor that connects the emitters and sensors to a control panel that is programmed to operate the emitters and sensors

wherein the placement of the graphene emitters produces a phased array effect when the emitters are activated and the touch-less EEG sensors measure brain wave patterns when the sensors are activated.

22. The TMS cap of claim 21 wherein the first configuration is a db emitter configuration and the second configuration is a yy emitter configuration.

23. A magnetic device comprising:

- a. a plurality of graphene magnetic emitters in a configuration that produces a phased array effect and
- b. at least one sensor.

24. The magnetic device of claim 23 wherein the emitters are two or more configurations.

25. The magnetic device of claim 24 wherein the emitters comprise db emitters and yy emitters.

26. A TMS device comprising a plurality of graphene magnetic emitters.

27. The TMS device of claim 26 further comprising a plurality of EEG sensors.

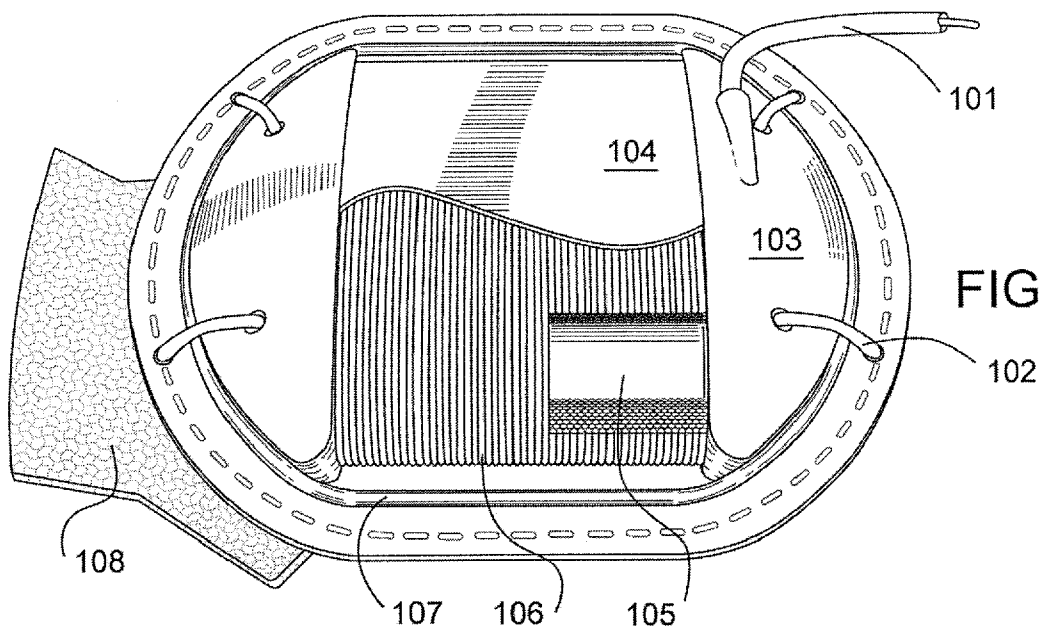


FIG. 1

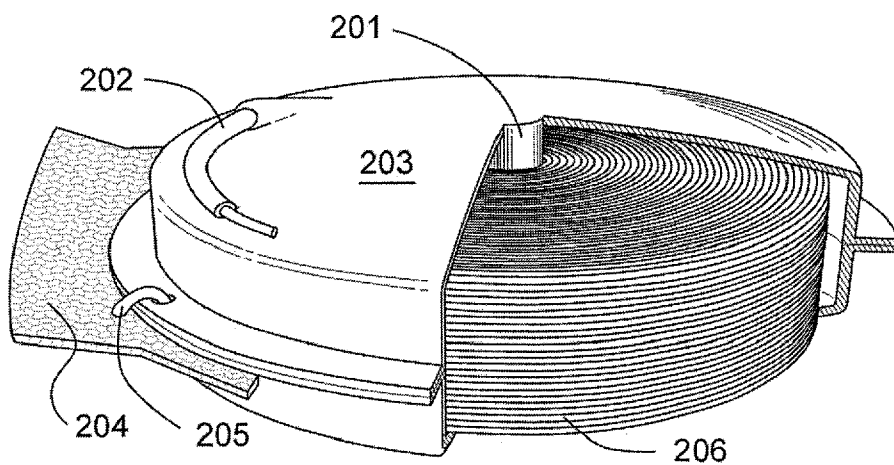


FIG. 2

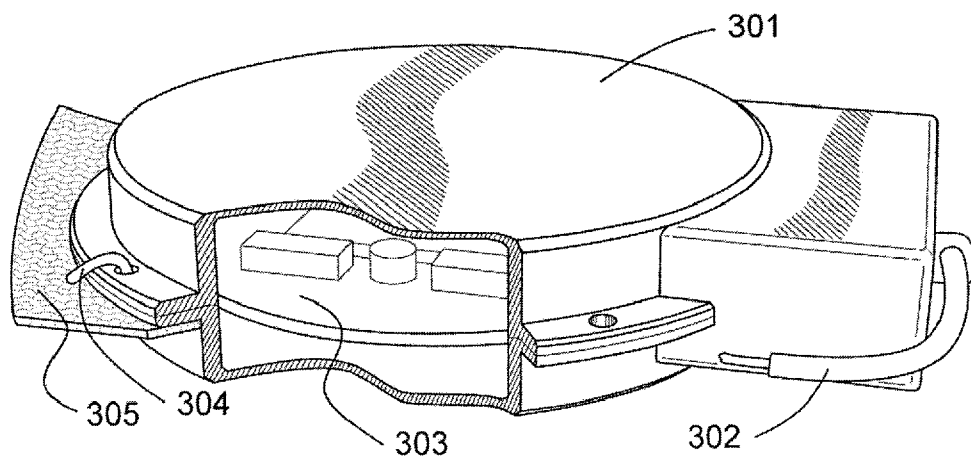


FIG. 3

FIG. 4

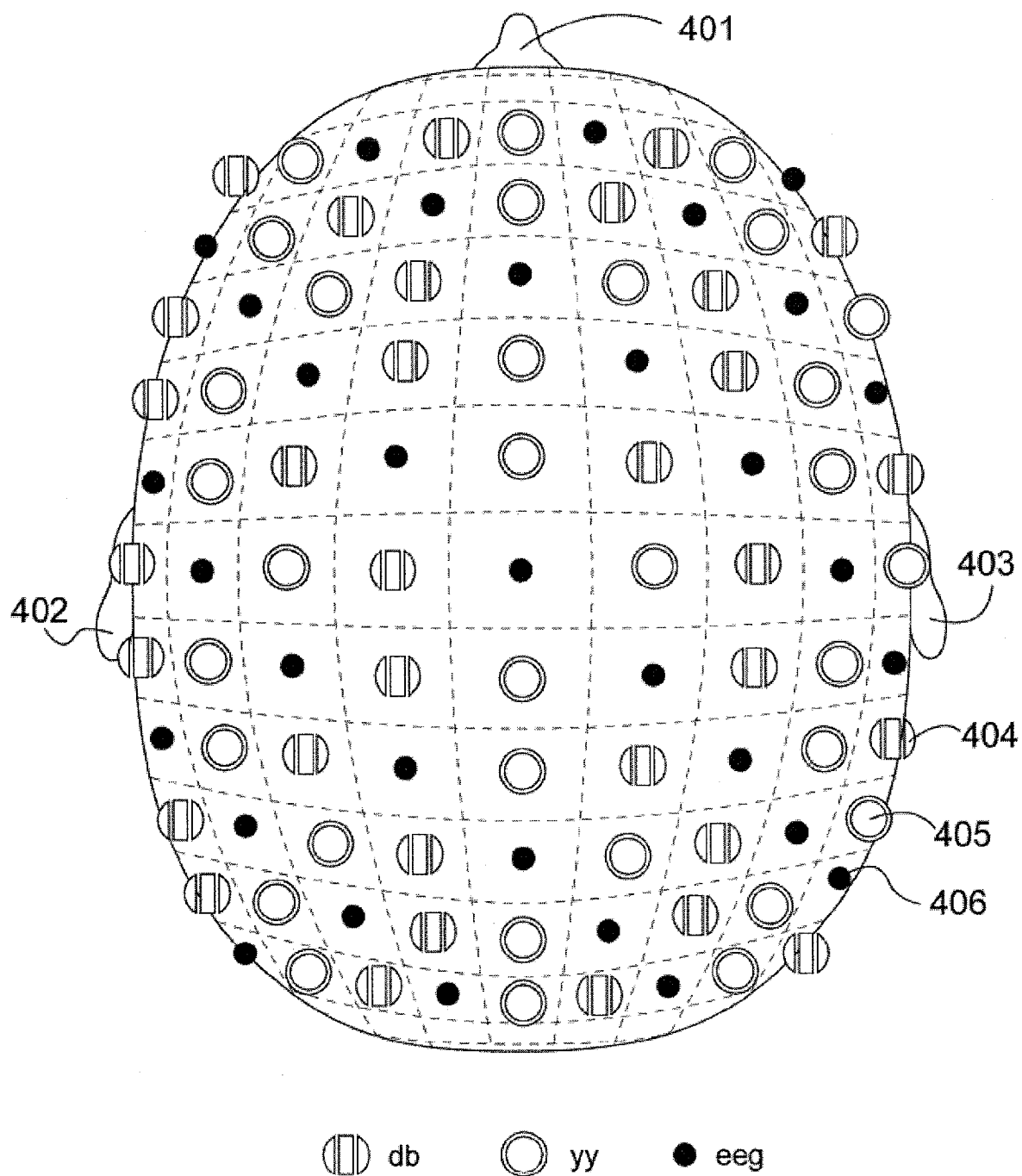


FIG. 5

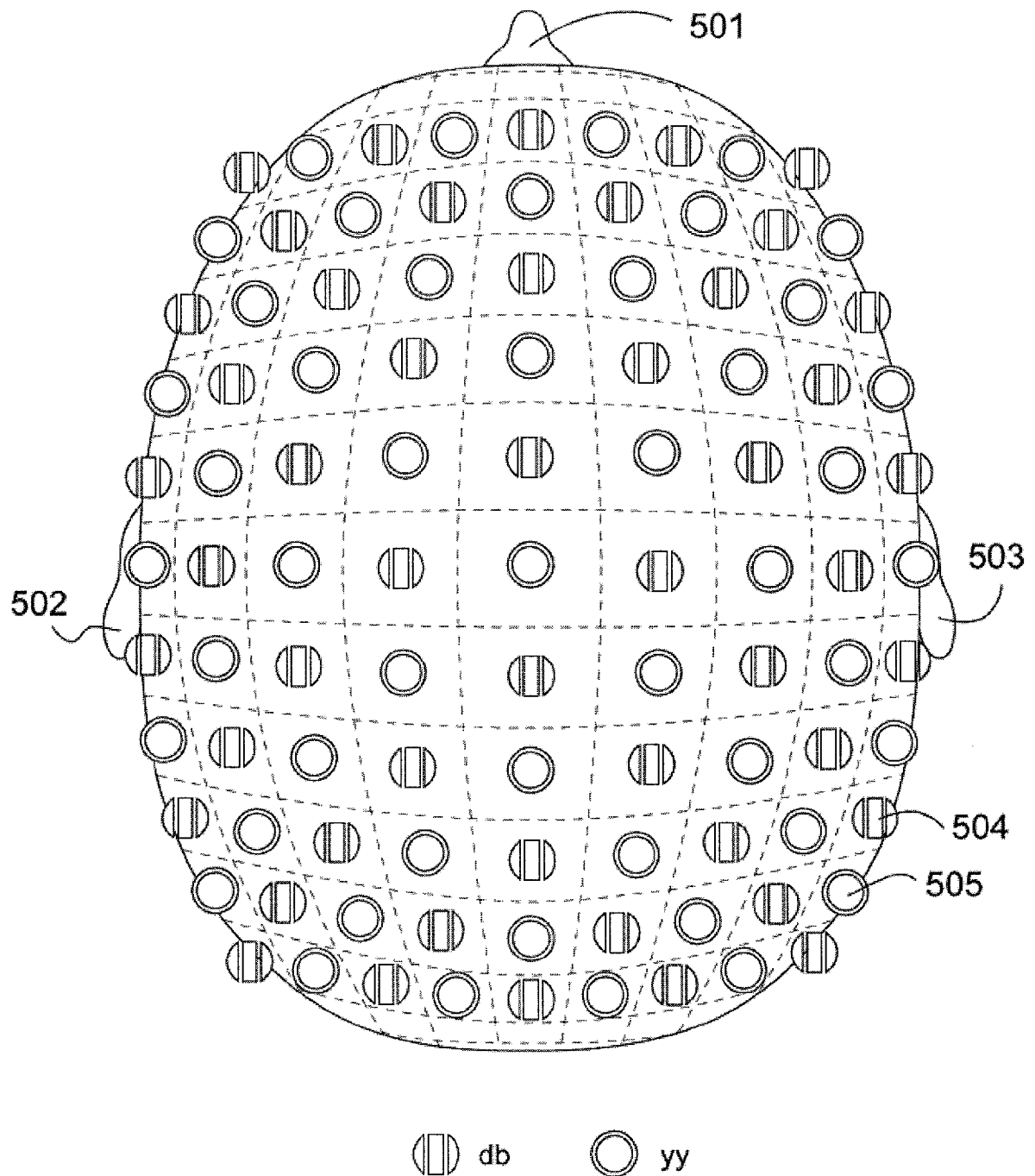


FIG. 6

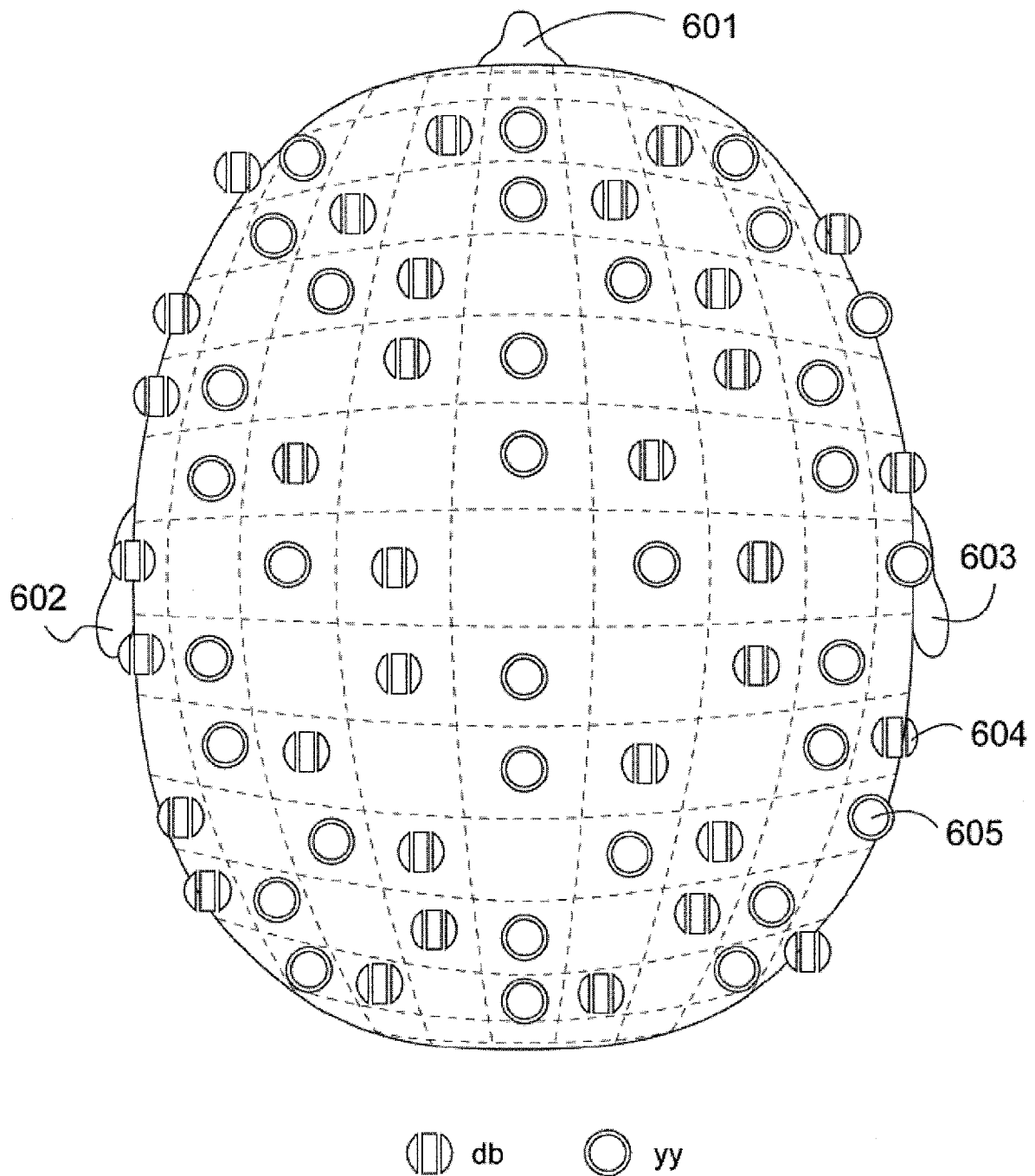


FIG. 7

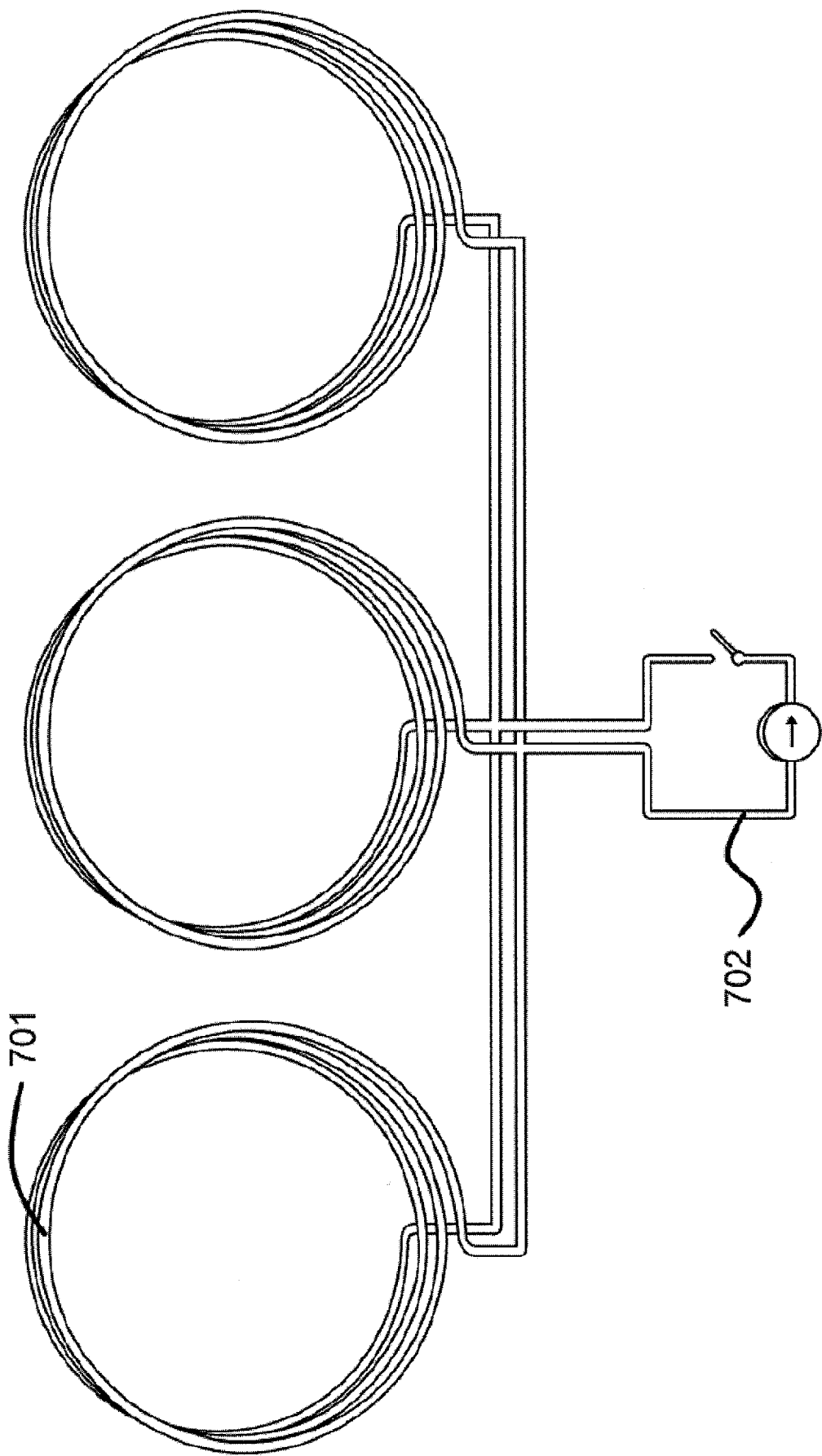
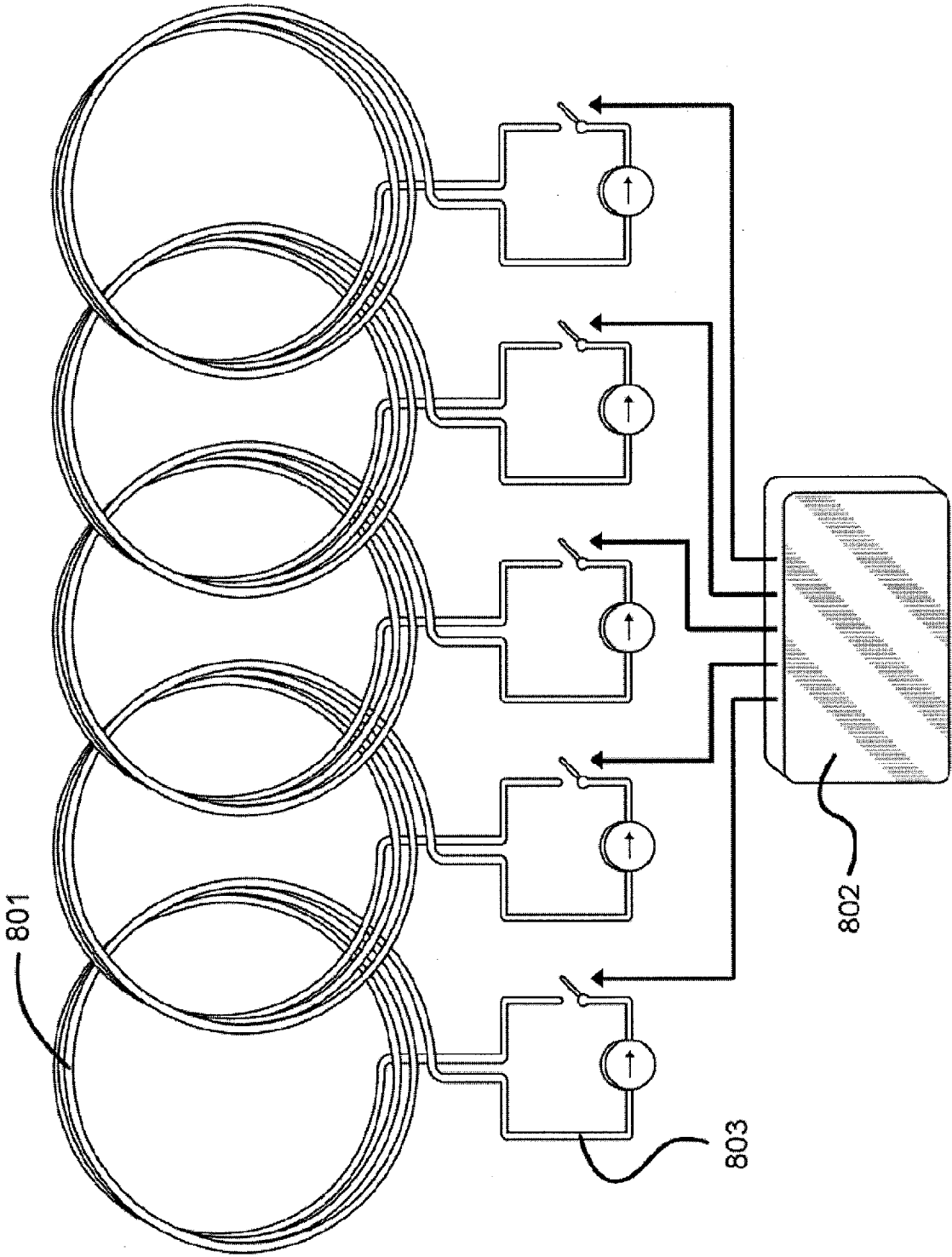


FIG. 8



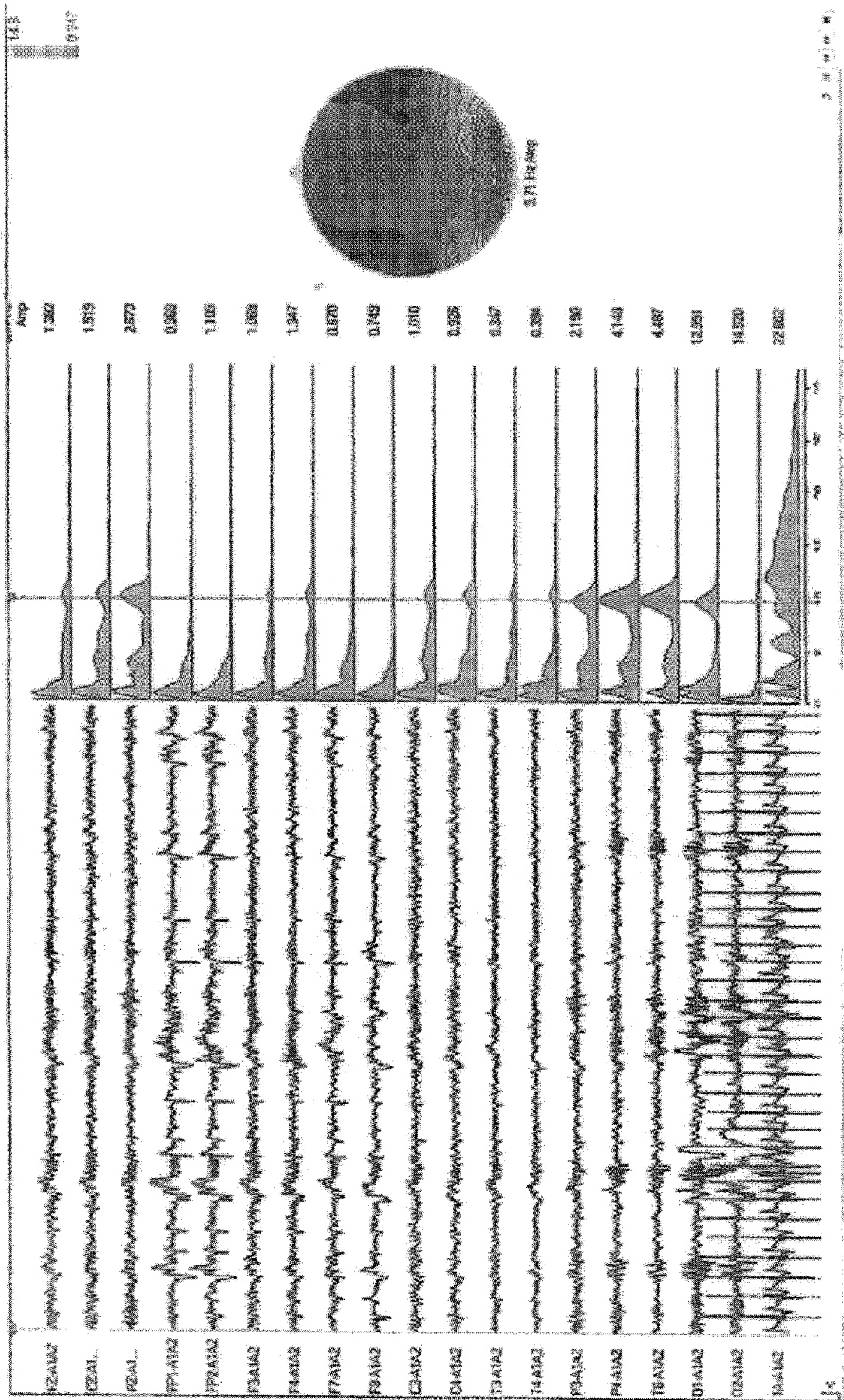


FIG. 9

FIG. 10a

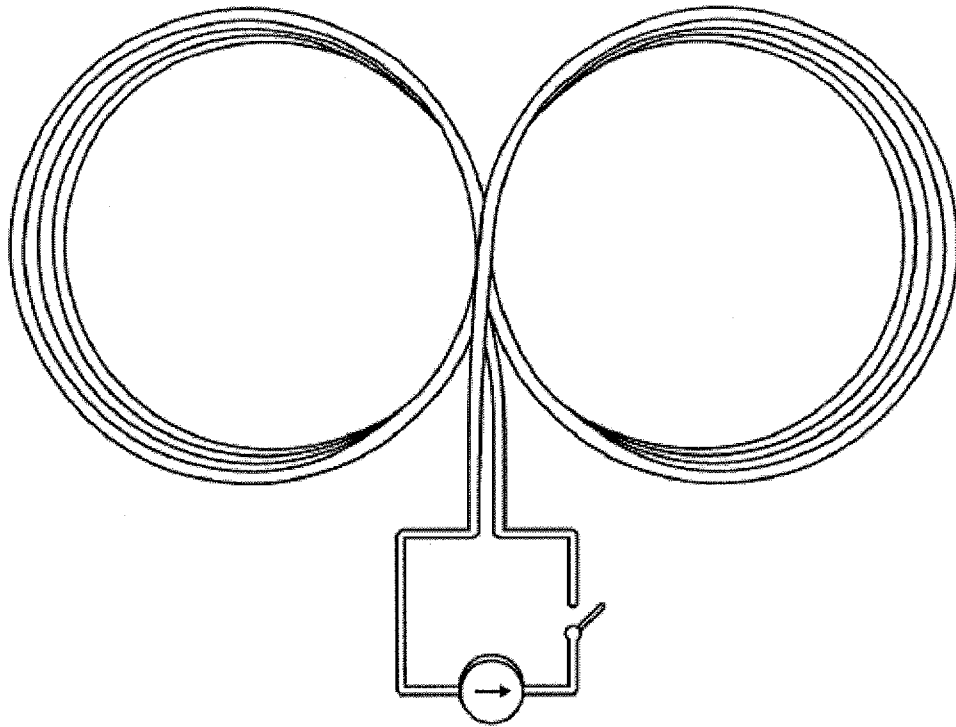
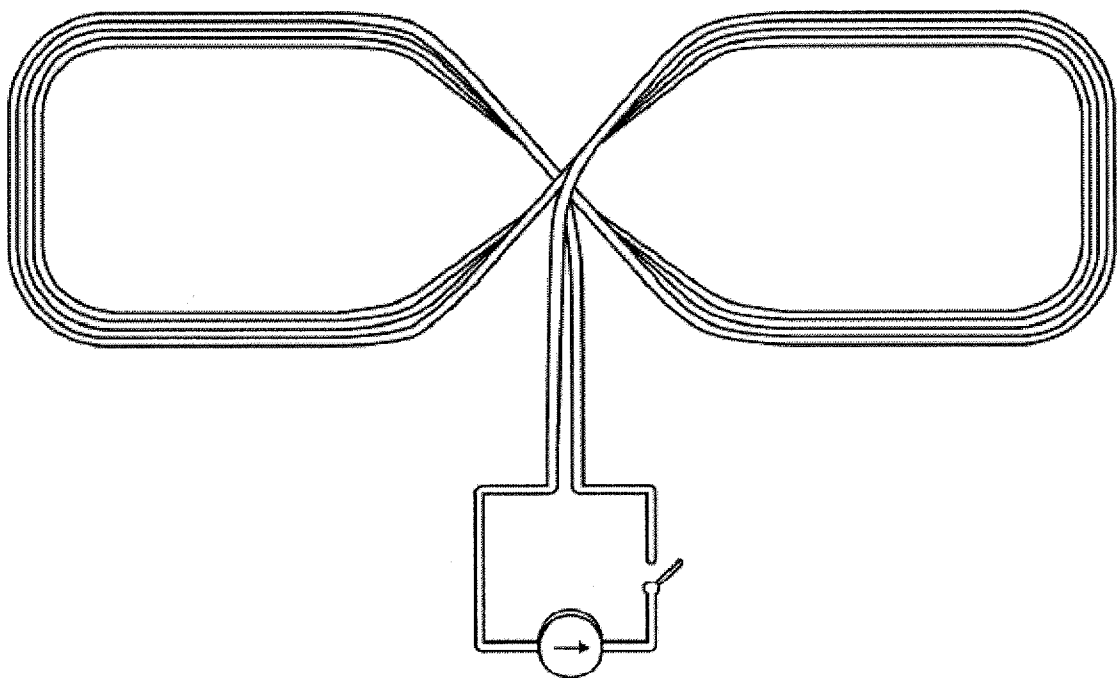


FIG. 10b



A. CLASSIFICATION OF SUBJECT MATTER**A61N 2/02(2006.01)i, A61B 5/0476(2006.01)i**

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

A61N 2/02; A61N 2/04; A61N 2/00; A61B 5/0476

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Korean utility models and applications for utility models

Japanese utility models and applications for utility models

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

eKOMPASS(KIPO internal) & Keywords: TMS, transcranial magnetic stimulation, graphene, magnetic, coil, electrode, array, configuration**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2011-0082326 A1 (MISHELEVICH, D. J. et al.) 7 April 2011. See abstract; claims 1,4-12,21,22,69; paragraphs [0009]-[0011], [0037], [0042]-[0044], [0055], [0058]-[0060], [0067], [0068]-[0070]; and figures 5-7.	1-8
A		13-27
Y	US 2010-0286470 A1 (SCHNEIDER, M. B. et al.) 11 November 2010. See abstract; claims 1-9,11-17,19; paragraphs [0013]-[0014], [0027]-[0031], [0068], [0072]; and figures 1A-4.	13, 16, 17, 19, 21, 23, 24, 26, 27
A		1-8, 14, 15, 18, 20, 22, 25
Y	Belle, D. "Graphene goes magnetic." nanotechweb.org. 17 November 2011. <URL = http://nanotechweb.org/cws/article/tech/47854 > See abstract.	13, 16, 17, 19, 21, 23, 24, 26, 27
A		1-8, 14, 15, 18, 20, 22, 25
A	US 2011-0319700 A1 (SCHNEIDER, M. B.) 29 December 2011. See abstract; claims 1,3,4,6-8; paragraphs [0011], [0013], [0016], [0018], [0022], [0025]-[0026], [0034]; and figure 1.	1-8, 13-27



Further documents are listed in the continuation of Box C.



See patent family annex.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

20 August 2013 (20.08.2013)

Date of mailing of the international search report

21 August 2013 (21.08.2013)

Name and mailing address of the ISA/KR

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INTERNATIONAL SEARCH REPORTInternational application No.
PCT/US2013/035664

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 2009-023680 A1 (NEOSTIM, INC.) 19 February 2009. See abstract; claims 1,4; paragraphs [0007]-[0009], [0013], [0016]-[0018]; and figures 1,3A,3B.	1-8,13-27

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US2013/035664

Box No. II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: 9-12
because they relate to subject matter not required to be searched by this Authority, namely:
Claims 9-12 pertain to methods for treatment of the human body and thus relate to a subject-matter which this International Searching Authority is not required, under Article 17(2)(a)(i) of the PCT and Rule 39.1(iv) of the Regulations under the PCT, to search.
2. ☐ Claims Nos.:
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:
3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box No. III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

- Invention 1 : A repetitive transcranial magnet stimulation device (claims 1-8).
Invention 2 : A magnetic device with graphene magnetic emitters (claims 13-27).

1. ☒ As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☒ The additional search fees were accompanied by the applicant's protest and, where applicable, the payment of a protest fee.
- ☐ The additional search fees were accompanied by the applicant's protest but the applicable protest fee was not paid within the time limit specified in the invitation.
- ☐ No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No.

PCT/US2013/035664

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2011-0082326 A1	07/04/2011	AU 2007-248790 A1 AU 2007-248790 B2 EP 2015843 A2 JP 2009-536073 A US 2005-0228209 A1 US 2007-0260107 A1 US 2009-0234243 A1 US 7520848 B2 US 8052591 B2 WO 2007-130308 A2	15/11/2007 01/12/2011 21/01/2009 08/10/2009 13/10/2005 08/11/2007 17/09/2009 21/04/2009 08/11/2011 15/11/2007
US 2010-0286470 A1	11/11/2010	AU 2008-288967 A1 CA 2694037 A1 EP 2183025 A1 JP 2010-536496 A US 2009-0099405 A1 US 2009-0156884 A1 US 2010-0185042 A1 US 2010-0256438 A1 US 2010-0298623 A1 US 8267850 B2 WO 2009-020938 A1 WO 2009-026386 A1 WO 2009-033144 A2 WO 2009-033150 A1 WO 2009-036040 A1 WO 2009-055634 A1	26/02/2009 20/02/2009 12/05/2010 02/12/2010 16/04/2009 18/06/2009 22/07/2010 07/10/2010 25/11/2010 18/09/2012 12/02/2009 26/02/2009 12/03/2009 12/03/2009 19/03/2009 30/04/2009
US 2011-0319700 A1	29/12/2011	None	
WO 2009-023680 A1	19/02/2009	US 2010-0256439 A1	07/10/2010

摘要

重复经颅磁刺激（rTMS）线圈或一组线圈被设计成利用同步磁场脉冲影响脑部的多个区域。公开了在感兴趣的目标区域上对准的多个线圈或以允许磁场影响感兴趣区域的形状拉伸或扩大的单个线圈。还公开了一种优化重复经颅磁磁极（rTMS）处理的方法。