



US008308045B2

(12) **United States Patent**
Bettuchi et al.

(10) **Patent No.:** **US 8,308,045 B2**
(45) **Date of Patent:** **Nov. 13, 2012**

(54) **ANNULAR ADHESIVE STRUCTURE**

(56) **References Cited**

(75) Inventors: **Michael J. Bettuchi**, Middletown, CT (US); **David N. Fowler**, Cheshire, CT (US); **Frank J. Viola**, Sandy Hook, CT (US); **Christopher J. Criscuolo**, Branford, CT (US); **Danyel J. Tarinelli**, Middletown, CT (US); **Robert Capella**, Shelton, CT (US); **Kevin Sniffin**, Danbury, CT (US); **Ahmad Robert Hadba**, Wallingford, CT (US)

U.S. PATENT DOCUMENTS

3,054,406	A	9/1962	Usher
3,124,136	A	3/1964	Usher
4,347,847	A	9/1982	Usher
4,354,628	A	10/1982	Green
4,452,245	A	6/1984	Usher
4,605,730	A	8/1986	Shalaby et al.
4,655,221	A	4/1987	Devereux
4,834,090	A	5/1989	Moore

(Continued)

(73) Assignee: **Tyco Healthcare Group LP**, Mansfield, MA (US)

FOREIGN PATENT DOCUMENTS

DE 1 99 24 311 A1 11/2000

(Continued)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 6 days.

OTHER PUBLICATIONS

(21) Appl. No.: **12/898,927**

International Search Report corresponding to European Application No. EP 06 00 4598, completed on Jun. 22, 2006; 2 pages.

(22) Filed: **Oct. 6, 2010**

(Continued)

(65) **Prior Publication Data**

US 2011/0024476 A1 Feb. 3, 2011

Primary Examiner — Lindsay Low

Related U.S. Application Data

(62) Division of application No. 11/248,846, filed on Oct. 12, 2005, now Pat. No. 7,823,592.

(60) Provisional application No. 60/620,268, filed on Oct. 18, 2004, provisional application No. 60/620,269, filed on Oct. 18, 2004, provisional application No. 60/620,066, filed on Oct. 18, 2004, provisional application No. 60/620,140, filed on Oct. 18, 2004, provisional application No. 60/669,104, filed on Apr. 7, 2005.

(51) **Int. Cl.**
A61B 17/115 (2006.01)

(52) **U.S. Cl.** **227/179.1**; 227/175.1; 227/19

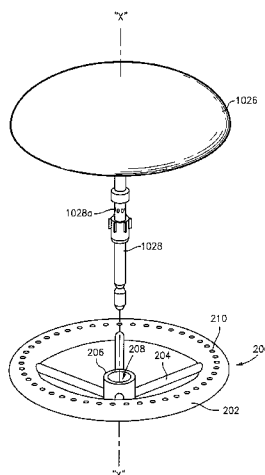
(58) **Field of Classification Search** 227/175.1–182.1, 227/19; 606/219

See application file for complete search history.

(57) **ABSTRACT**

An apparatus for forming an anastomosis between adjacent intestinal sections of tissue is provided. The apparatus includes a circular surgical stapler having an anvil assembly with an anvil shaft and an anvil, the circular surgical stapler further having a tubular body portion with an annular knife and a body portion shaft selectively attachable to the anvil shaft; and a seal structure for deposition between the intestinal sections of tissue including a hub configured to engage attachment structure on at least one of the anvil shaft and the body portion shaft. The attachment structure is positioned so that the seal structure is located between the intestinal sections of tissue when the circular surgical stapler is disposed within the intestinal sections of tissue.

8 Claims, 22 Drawing Sheets



U.S. PATENT DOCUMENTS				
4,838,884 A	6/1989	Dumican et al.	6,677,258 B2	1/2004 Carroll et al.
4,930,674 A	6/1990	Barak	6,685,714 B2	2/2004 Rousseau
5,002,551 A	3/1991	Linsky et al.	6,704,210 B1	3/2004 Myers
5,014,899 A	5/1991	Presty et al.	6,723,114 B2	4/2004 Shalaby
5,040,715 A	8/1991	Green et al.	6,726,706 B2	4/2004 Dominguez
5,065,929 A	11/1991	Schulze et al.	6,736,823 B2	5/2004 Darois et al.
5,205,459 A	4/1993	Brinkerhoff et al.	6,736,854 B2	5/2004 Vadurro et al.
5,222,963 A	6/1993	Brinkerhoff et al.	6,746,458 B1	6/2004 Cloud
5,238,026 A	8/1993	Goto	6,773,458 B1	8/2004 Brauker et al.
5,263,629 A	11/1993	Trumbull et al.	6,927,315 B1	8/2005 Heinecke et al.
5,314,471 A	5/1994	Brauker et al.	7,128,748 B2	10/2006 Mooradian et al.
5,344,454 A	9/1994	Clarke et al.	7,147,138 B2	12/2006 Shelton, IV
5,392,979 A	2/1995	Green et al.	7,431,730 B2	10/2008 Viola
5,397,324 A	3/1995	Carroll et al.	7,434,717 B2	10/2008 Shelton, IV et al.
5,425,745 A	6/1995	Green et al.	7,438,209 B1	10/2008 Hess et al.
5,441,193 A	8/1995	Gravener	7,547,312 B2	6/2009 Bauman et al.
5,441,507 A	8/1995	Wilk et al.	7,559,937 B2	7/2009 de la Torre et al.
5,468,253 A	11/1995	Bezswana et al.	7,604,151 B2	10/2009 Hess et al.
5,503,638 A	4/1996	Cooper et al.	7,665,646 B2	2/2010 Prommersberger
5,542,594 A	8/1996	McKean et al.	7,744,627 B2	6/2010 Orban, III et al.
5,549,628 A	8/1996	Cooper et al.	7,793,813 B2	9/2010 Bettuchi
5,575,803 A	11/1996	Cooper et al.	7,823,592 B2	11/2010 Bettuchi et al.
5,653,756 A	8/1997	Clarke et al.	7,845,533 B2	12/2010 Marczyk et al.
5,683,809 A	11/1997	Freeman et al.	7,845,536 B2	12/2010 Viola et al.
5,690,675 A	11/1997	Sawyer et al.	7,909,224 B2	3/2011 Prommersberger
5,702,409 A	12/1997	Rayburn et al.	2002/0016626 A1	2/2002 DiMatteo et al.
5,752,965 A	5/1998	Francis et al.	2002/0019187 A1	2/2002 Carroll et al.
5,762,256 A	6/1998	Mastri et al.	2002/0052622 A1	5/2002 Rousseau
5,766,188 A	6/1998	Igaki	2002/0091397 A1	7/2002 Chen
5,769,892 A	6/1998	Kingwell	2002/0133236 A1	9/2002 Rousseau
5,782,396 A	7/1998	Mastri et al.	2002/0138152 A1	9/2002 Francis et al.
5,799,857 A	9/1998	Robertson et al.	2002/0151911 A1	10/2002 Gabbay
5,810,855 A	9/1998	Rayburn et al.	2002/0165559 A1	11/2002 Grant et al.
5,814,057 A	9/1998	Oi et al.	2002/0165562 A1	11/2002 Grant et al.
5,833,695 A	11/1998	Yoon	2002/0165563 A1	11/2002 Grant et al.
5,843,096 A	12/1998	Igaki et al.	2002/0177859 A1	11/2002 Monassevitch et al.
5,895,412 A	4/1999	Tucker	2003/0065345 A1	4/2003 Weadock
5,895,415 A	4/1999	Chow et al.	2003/0065346 A1	4/2003 Evens et al.
5,902,312 A	5/1999	Frater et al.	2003/0083676 A1	5/2003 Wallace
5,908,427 A	6/1999	McKean et al.	2003/0088256 A1	5/2003 Conston et al.
5,915,616 A	6/1999	Viola et al.	2003/0105510 A1	6/2003 DiMatteo et al.
5,931,847 A	8/1999	Bittner et al.	2003/0114866 A1	6/2003 Ulmsten et al.
5,964,774 A	10/1999	McKean et al.	2003/0120284 A1	6/2003 Palacios
5,997,895 A	12/1999	Narotam et al.	2003/0167064 A1	9/2003 Whayne
6,019,791 A	2/2000	Wood	2003/0181927 A1	9/2003 Wallace
6,030,392 A	2/2000	Dakov et al.	2003/0183671 A1	10/2003 Mooradian et al.
6,032,849 A	3/2000	Mastri et al.	2003/0208231 A1	11/2003 Williamson, IV et al.
6,045,560 A	4/2000	McKean et al.	2004/0034377 A1	2/2004 Sharkawy et al.
6,063,097 A	5/2000	Oi et al.	2004/0092960 A1	5/2004 Abrams et al.
6,080,169 A	6/2000	Turtel	2004/0093029 A1	5/2004 Zubik et al.
6,099,551 A	8/2000	Gabbay	2004/0107006 A1	6/2004 Francis et al.
6,149,667 A	11/2000	Hovland et al.	2004/0116945 A1	6/2004 Sharkawy et al.
6,155,265 A	12/2000	Hammerslag	2004/0142621 A1	7/2004 Carroll et al.
6,165,185 A	12/2000	Shennib et al.	2004/0172048 A1	9/2004 Browning
6,210,439 B1	4/2001	Firmin et al.	2004/0209059 A1	10/2004 Foss
6,214,020 B1	4/2001	Mulhauser et al.	2004/0215214 A1	10/2004 Crews et al.
6,241,139 B1	6/2001	Milliman et al.	2004/0215219 A1	10/2004 Eldridge et al.
6,258,107 B1	7/2001	Balazs et al.	2004/0215221 A1	10/2004 Suyker et al.
6,267,772 B1	7/2001	Mulhauser et al.	2004/0254590 A1	12/2004 Hoffman et al.
6,273,897 B1	8/2001	Dalessandro et al.	2004/0260315 A1	12/2004 Dell et al.
6,280,453 B1	8/2001	Kugel et al.	2005/0002981 A1	1/2005 Lahtinen et al.
6,299,631 B1	10/2001	Shalaby	2005/0021026 A1	1/2005 Bailly
6,312,457 B1	11/2001	DiMatteo et al.	2005/0021053 A1	1/2005 Heinrich
6,312,474 B1	11/2001	Francis et al.	2005/0021085 A1	1/2005 Abrams et al.
6,325,810 B1	12/2001	Hamilton et al.	2005/0059996 A1	3/2005 Bauman et al.
6,436,030 B2	8/2002	Rehil	2005/0059997 A1	3/2005 Bauman et al.
6,454,780 B1	9/2002	Wallace	2005/0070929 A1	3/2005 Dalessandro et al.
6,461,368 B2	10/2002	Fogarty et al.	2005/0118435 A1	6/2005 DeLucia et al.
6,503,257 B2	1/2003	Grant et al.	2005/0228446 A1	10/2005 Mooradian et al.
6,503,259 B2	1/2003	Huxel et al.	2005/0245965 A1	11/2005 Orban et al.
6,514,283 B2	2/2003	DiMatteo et al.	2006/0004407 A1	1/2006 Hiles et al.
6,517,566 B1	2/2003	Hovland et al.	2006/0085034 A1	4/2006 Bettuchi
6,551,356 B2	4/2003	Rousseau	2006/0135992 A1	6/2006 Bettuchi et al.
6,592,597 B2	7/2003	Grant et al.	2006/0173470 A1	8/2006 Oray et al.
6,638,285 B2	10/2003	Gabbay	2006/0178683 A1	8/2006 Shimoji et al.
6,652,594 B2	11/2003	Francis et al.	2006/0212050 A1	9/2006 D'Agostino et al.
6,656,193 B2	12/2003	Grant et al.	2006/0271104 A1	11/2006 Viola et al.
6,669,735 B1	12/2003	Pelissier	2007/0034669 A1	2/2007 de la Torre et al.
			2007/0049953 A2	3/2007 Shimoji et al.

2007/0179528	A1	8/2007	Soltz et al.
2007/0203509	A1	8/2007	Bettuchi
2007/0203510	A1	8/2007	Bettuchi
2007/0246505	A1	10/2007	Pace-Florida et al.
2008/0029570	A1	2/2008	Shelton et al.
2008/0082126	A1	4/2008	Murray et al.
2008/0110959	A1	5/2008	Orban et al.
2008/0125812	A1	5/2008	Zubik et al.
2008/0140115	A1	6/2008	Stopek
2008/0161831	A1	7/2008	Bauman et al.
2008/0161832	A1	7/2008	Bauman et al.
2008/0169327	A1	7/2008	Shelton et al.
2008/0169328	A1	7/2008	Shelton
2008/0169329	A1	7/2008	Shelton et al.
2008/0169330	A1	7/2008	Shelton et al.
2008/0169331	A1	7/2008	Shelton et al.
2008/0169332	A1	7/2008	Shelton et al.
2008/0169333	A1	7/2008	Shelton et al.
2008/0290134	A1	11/2008	Bettuchi et al.
2008/0308608	A1	12/2008	Prommersberger
2008/0314960	A1	12/2008	Marczyk et al.
2009/0001121	A1	1/2009	Hess et al.
2009/0001122	A1	1/2009	Prommersberger et al.
2009/0001123	A1	1/2009	Morgan et al.
2009/0001124	A1	1/2009	Hess et al.
2009/0001125	A1	1/2009	Hess et al.
2009/0001126	A1	1/2009	Hess et al.
2009/0001128	A1	1/2009	Weisenburgh, II et al.
2009/0001130	A1	1/2009	Hess et al.
2009/0005808	A1	1/2009	Hess et al.
2009/0030452	A1	1/2009	Bauman et al.
2009/0043334	A1	2/2009	Bauman et al.
2009/0078739	A1	3/2009	Viola
2009/0095791	A1	4/2009	Eskaros et al.
2009/0095792	A1	4/2009	Bettuchi
2009/0120994	A1	5/2009	Murray et al.
2009/0134200	A1	5/2009	Tarinelli et al.
2009/0206125	A1	8/2009	Huitema et al.
2009/0206126	A1	8/2009	Huitema et al.
2009/0206139	A1	8/2009	Hall et al.
2009/0206141	A1	8/2009	Huitema et al.
2009/0206142	A1	8/2009	Huitema et al.
2009/0206143	A1	8/2009	Huitema et al.
2009/0218384	A1	9/2009	Aranyi
2009/0277947	A1	11/2009	Viola
2009/0287230	A1	11/2009	D'Agostino et al.
2010/0012704	A1	1/2010	Tarinelli Racenet et al.
2010/0065606	A1	3/2010	Stopek
2010/0065607	A1	3/2010	Orban, III et al.
2010/0072254	A1	3/2010	Aranyi et al.
2010/0147921	A1	6/2010	Olson
2010/0147922	A1	6/2010	Olson
2010/0147923	A1	6/2010	D'Agostino et al.
2010/0243707	A1	9/2010	Olson et al.
2010/0243708	A1	9/2010	Aranyi et al.
2010/0243711	A1	9/2010	Olson et al.
2010/0249805	A1	9/2010	Olson et al.
2010/0264195	A1	10/2010	Bettuchi
2010/0282815	A1	11/2010	Bettuchi et al.
2011/0024476	A1	2/2011	Bettuchi et al.
2011/0024481	A1	2/2011	Bettuchi et al.
2011/0036894	A1	2/2011	Bettuchi
2011/0042442	A1	2/2011	Viola et al.
2011/0046650	A1	2/2011	Bettuchi
2011/0057016	A1	3/2011	Bettuchi

FOREIGN PATENT DOCUMENTS

DE	199 24 311	A1	11/2000
EP	0 594 148		4/1994
EP	0 594 148	A1	4/1994
EP	0 327 022	B1	4/1995
EP	0 667 119	A1	8/1995
EP	1 064 883	A1	1/2001
EP	1 256 317	A2	11/2002
EP	1 306 061	A2	5/2003

EP	1 520 525		4/2005
EP	1 520 525	A1	4/2005
EP	1 621 141	A21	2/2006
EP	1 759 640	A2	3/2007
EP	2 005 894	A2	12/2008
EP	2 005 895	A2	12/2008
JP	06327683	A	11/1994
WO	WO 90/05489		5/1990
WO	WO 90/05489	A1	5/1990
WO	WO 97/01989	A1	1/1997
WO	WO 97/13463		4/1997
WO	WO 98/17180		4/1998
WO	WO 98/17180	A1	4/1998
WO	WO 99/45849		9/1999
WO	WO 99/45849	A1	9/1999
WO	WO 03/082126	A1	10/2003
WO	WO 03094746	A1	11/2003
WO	WO 03/105698	A2	12/2003
WO	WO 03/206698	A2	12/2003
WO	WO 2006/023578		3/2006
WO	WO 2006/023578	A2	3/2006
WO	WO 2006/044490		4/2006
WO	WO 2006/044490	A2	4/2006
WO	WO 2006/083748	A1	8/2006
WO	WO 2008/057281	A2	5/2008
WO	WO 2008/109125	A1	9/2008

OTHER PUBLICATIONS

International Search Report corresponding to European Application No. EP 06 01 6962.0, completed on Jan. 3, 2007 and mailed on Jan. 11, 2007; 10 pages.

International Search Report corresponding to International Application No. PCT/US05/36740, completed on Feb. 20, 2007 and mailed on Mar. 23, 2007; 8 pages.

International Search Report corresponding to International Application No. PCT/US2008/002981, completed on Jun. 9, 2008 and mailed on Jun. 26, 2008; 2 pages.

International Search Report corresponding to European Application No. EP08 25 1779, completed on Jul. 14, 2008 and mailed on Jul. 23, 2008; 5 pages.

International Search Report corresponding to European Application No. EP 08 25 1989.3, completed on Mar. 11, 2010 and mailed on Mar. 24, 2010; 3 pages.

International Search Report corresponding to European Application No. EP 10 25 1437.9, completed on Nov. 22, 2010 and mailed on Dec. 16, 2010; 3 pages.

International Search Report corresponding to European Application No. EP 09 25 2897.5, completed on Feb. 7, 2011 and mailed on Feb. 15, 2011; 3 pages.

International Search Report for PCT/US05/35120 date of completion is May 6, 2008 (10 pages).

European Search Report for EP05803193.1-2310 date of completion is Feb. 9, 2010 (3 pages).

International Search Report for EP 08 25 1779 dated Jul. 23, 2008.

International Search Report for EP 06016962.0 dated Jan. 3, 2007.

International Search Report for PCT/US05/36740 date of completion is Mar. 23, 2007 (2 pages).

International Search Report for PCT/US2008/002981 dated Jun. 26, 2008.

International Search Report corresponding to European Application No. EP 10 25 0715.9, completed on Jun. 30, 2010 and mailed on Jul. 20, 2010; 3 pages.

International Search Report corresponding to European Application No. EP 10 25 0642.5, completed on Mar. 25, 2011 and mailed on Apr. 4, 2011; 4 pages.

European Search Report for corresponding EP05 80 4382, date of completion is Oct. 5, 2010 (3 pages).

European Search Report for EP 11164908.3-2310 date of completion is Jan. 5, 2012 (7 pages).

European Search Report for EP 12150511.9.3-2310 date of completion is Apr. 16, 2012 (7 pages).

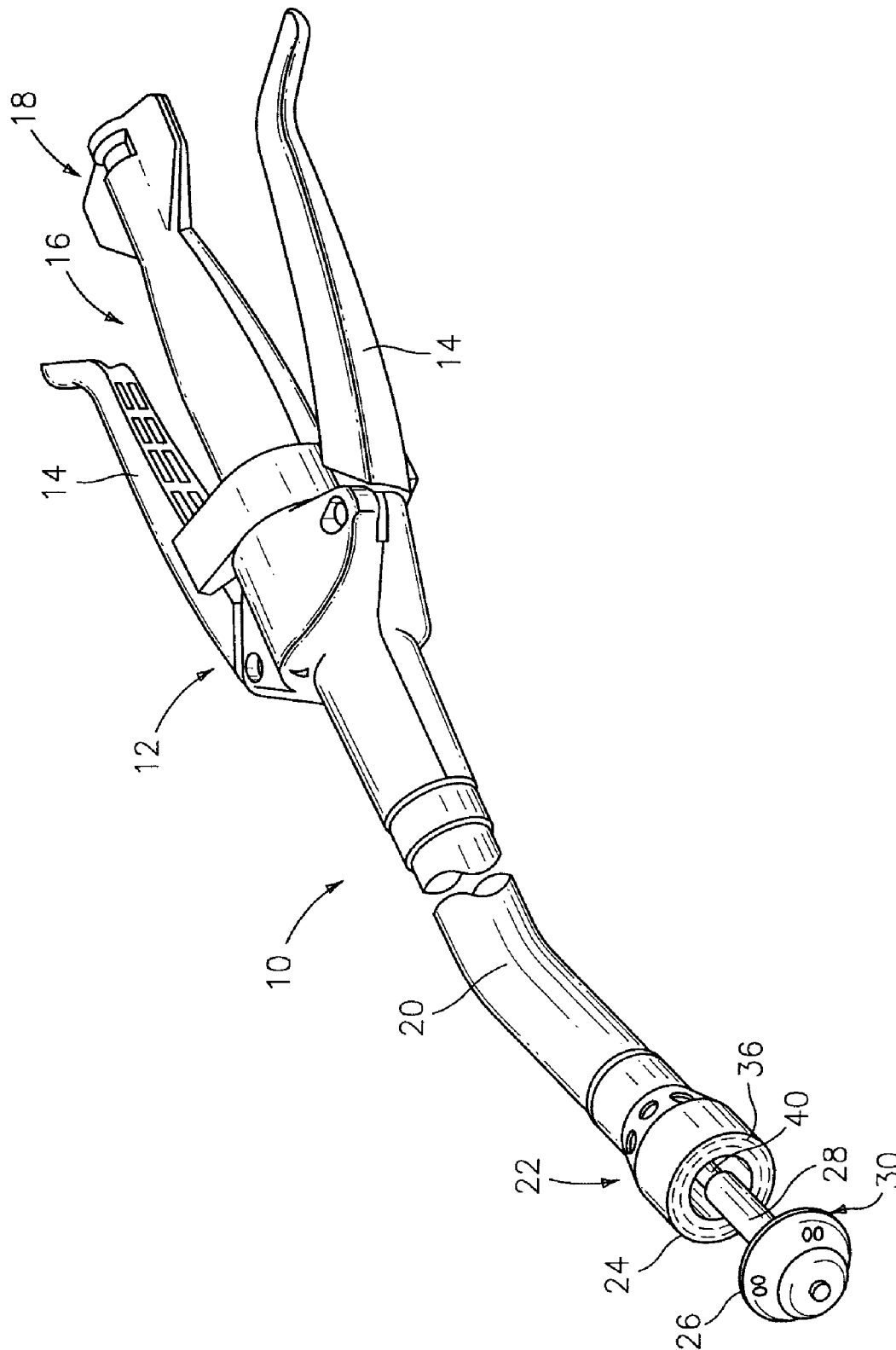


FIG. 1

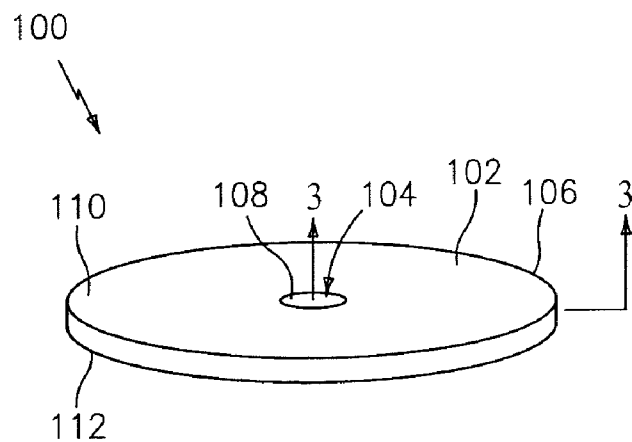


FIG. 2

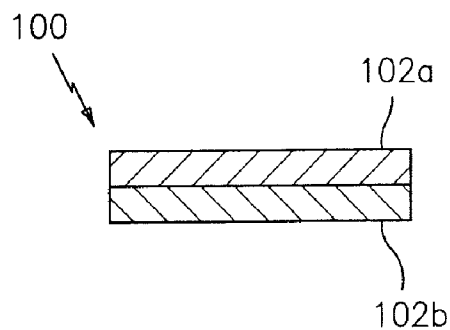


FIG. 3

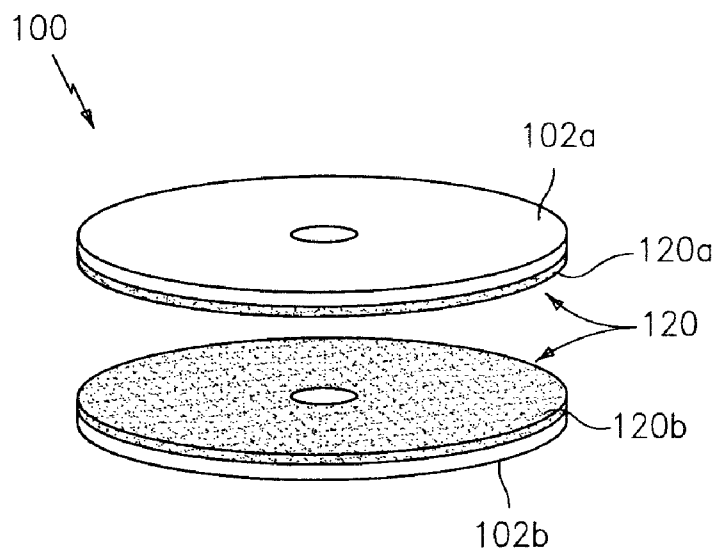


FIG. 4

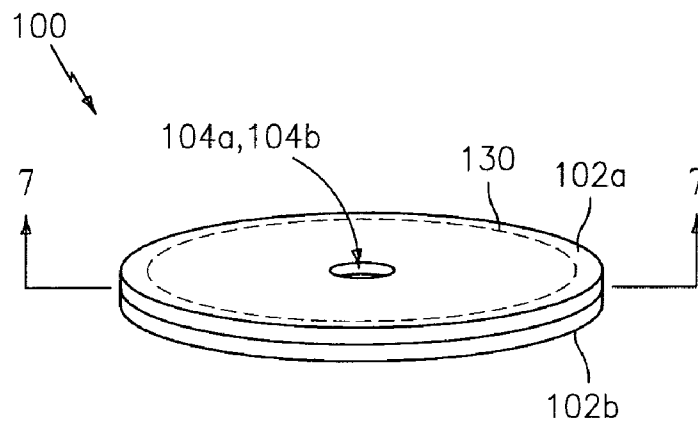


FIG. 5

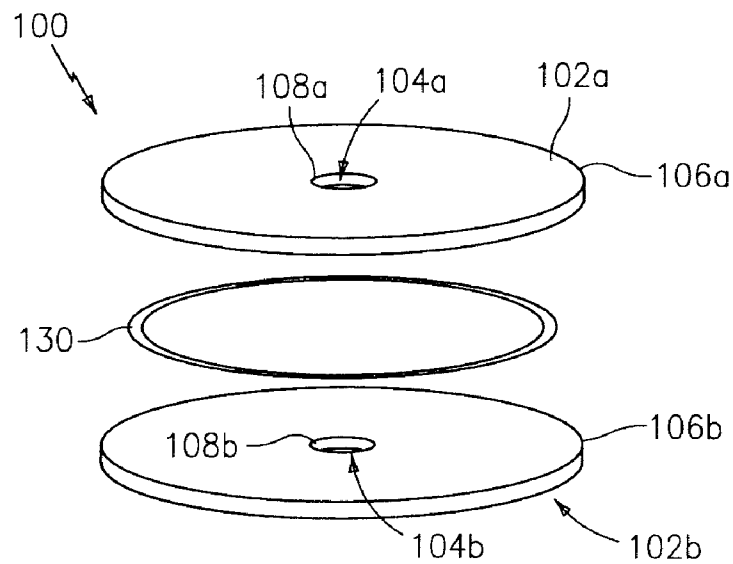


FIG. 6

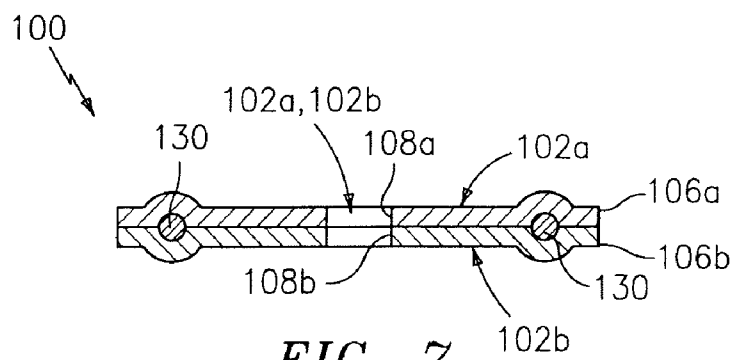


FIG. 7

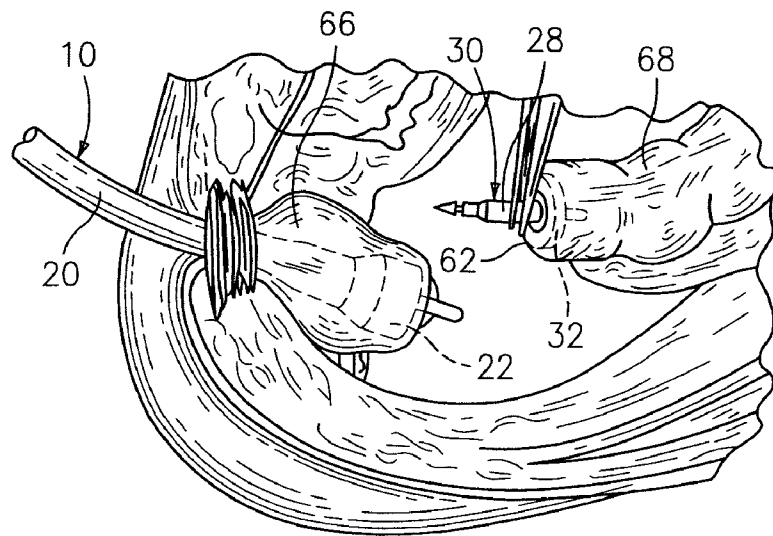


FIG. 8

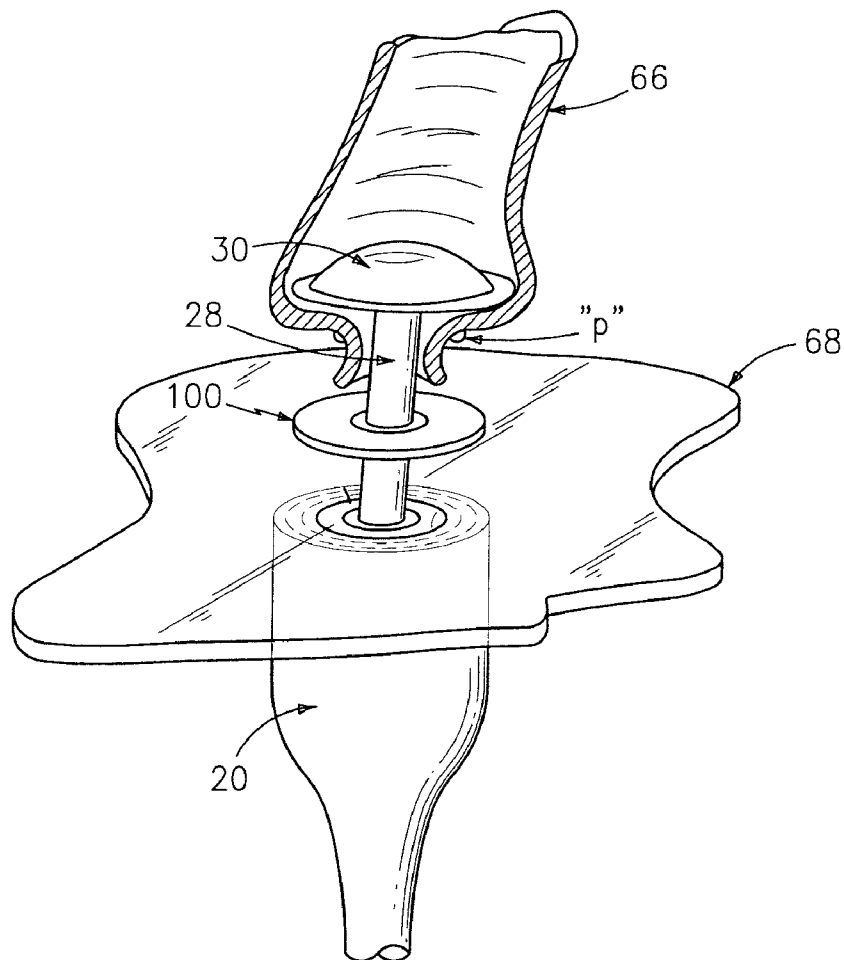


FIG. 9

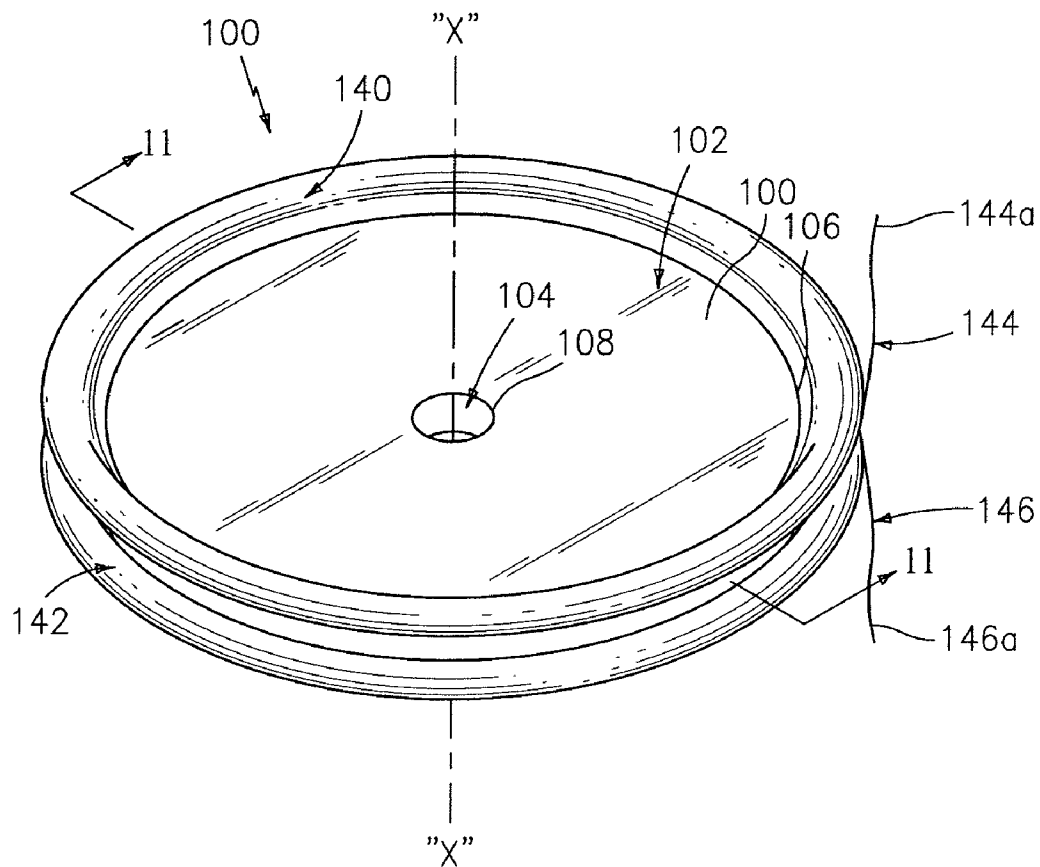


FIG. 10

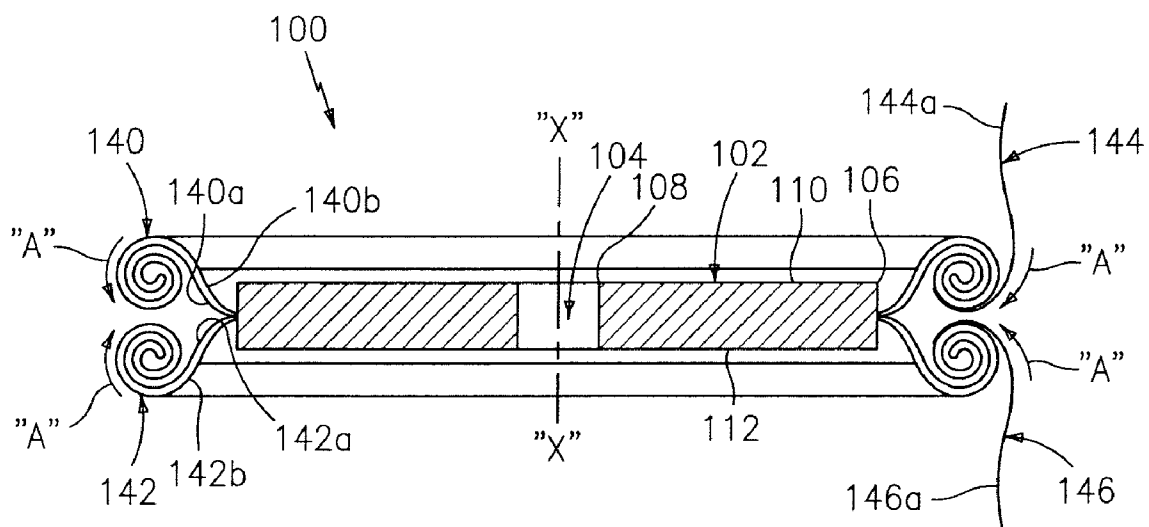


FIG. 11

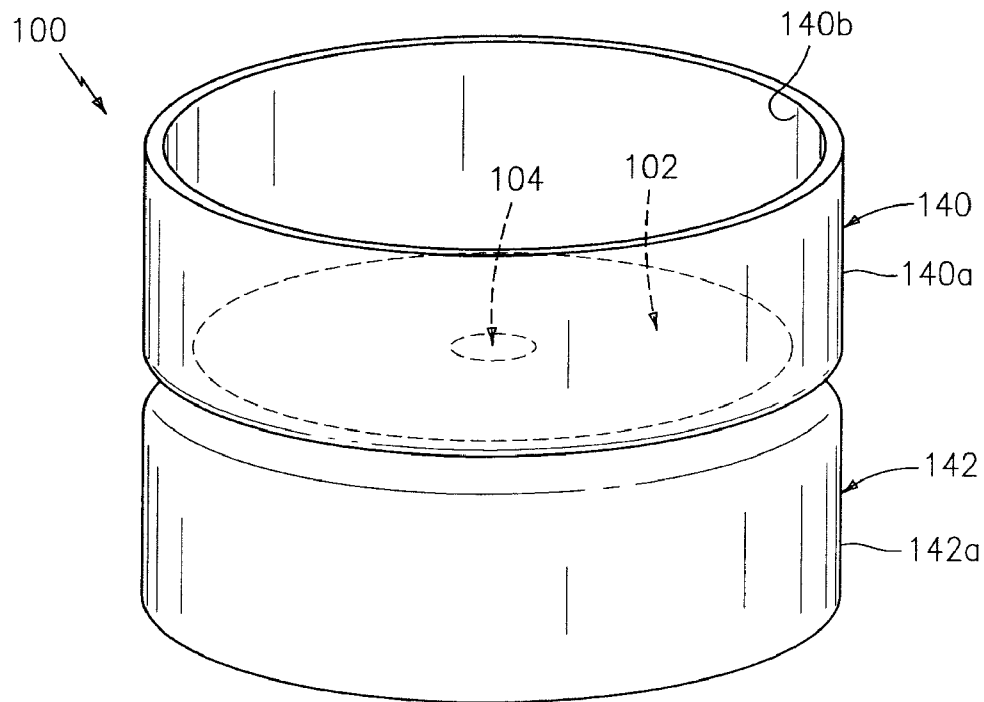


FIG. 12

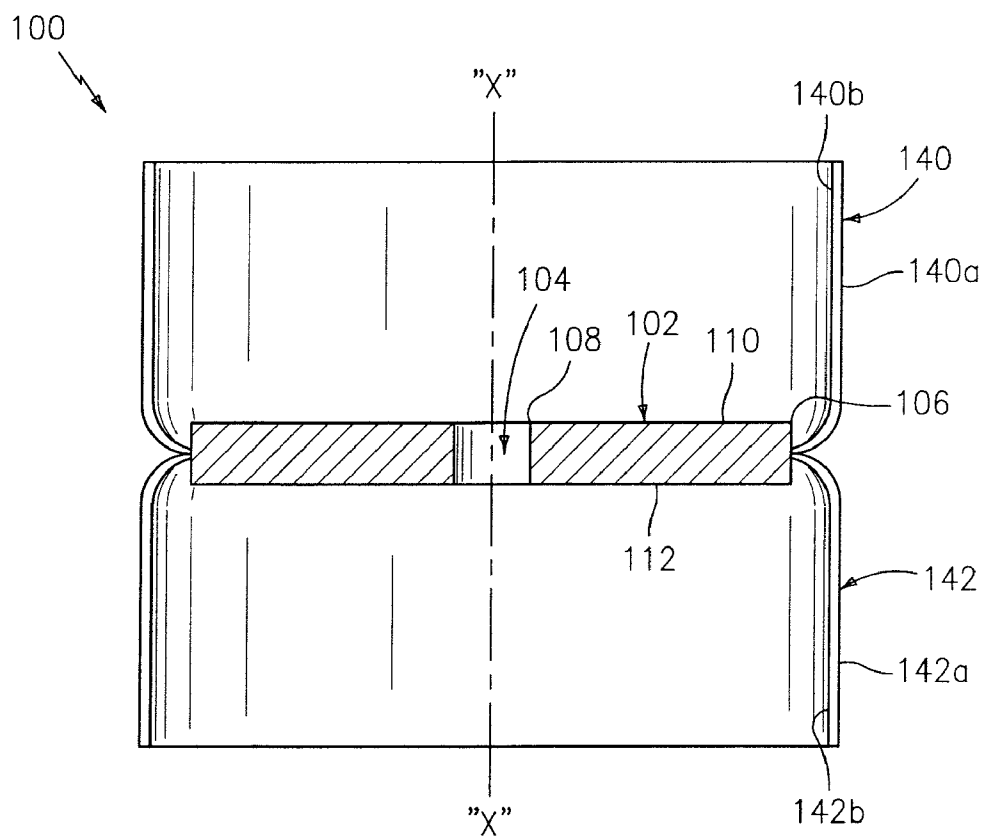


FIG. 13

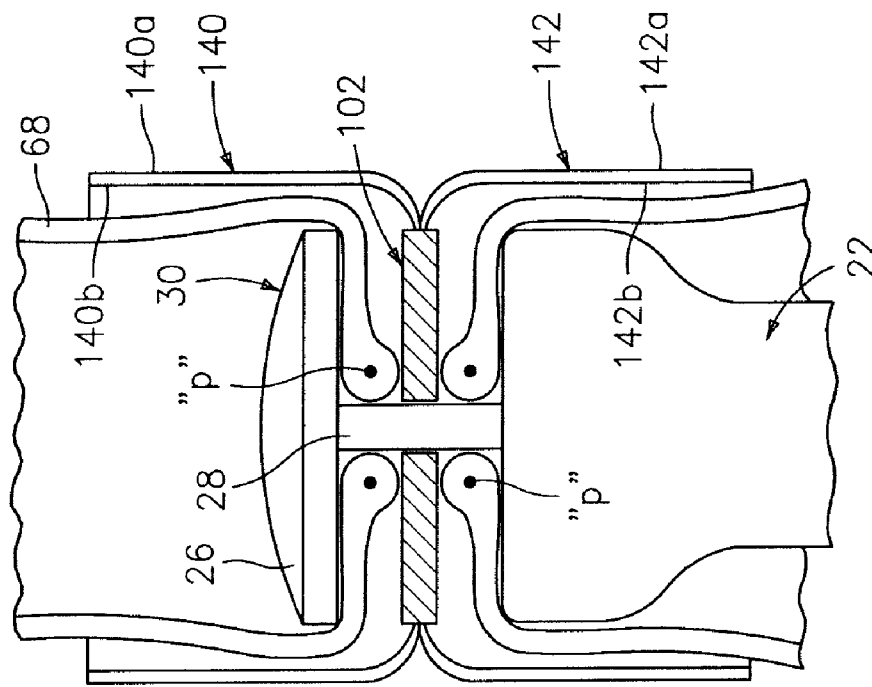


FIG. 15

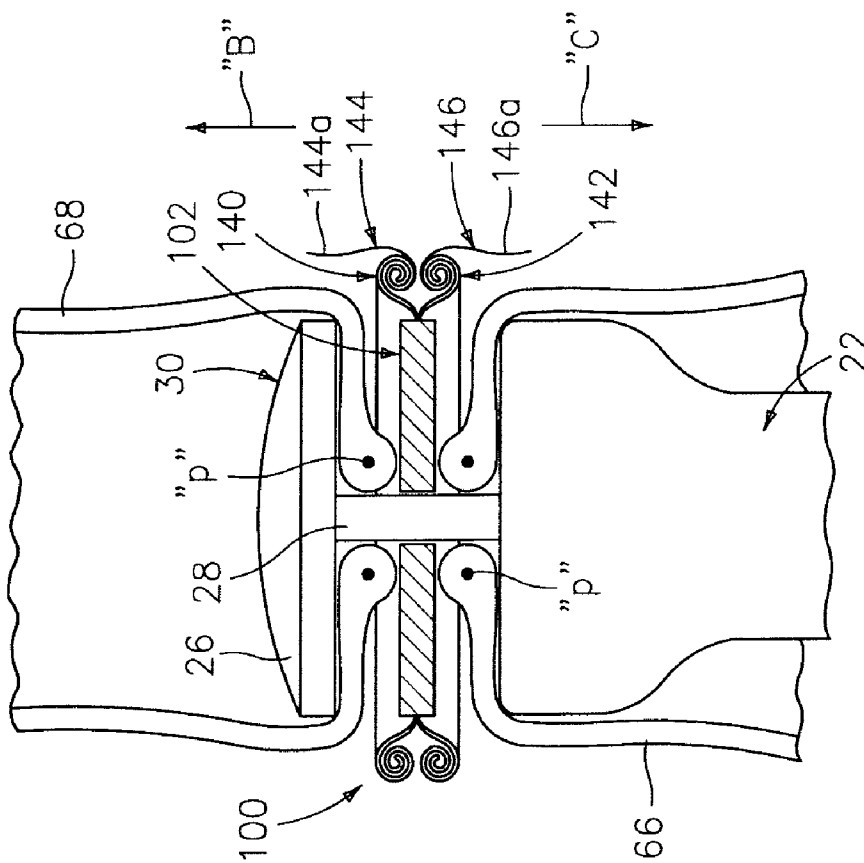


FIG. 14

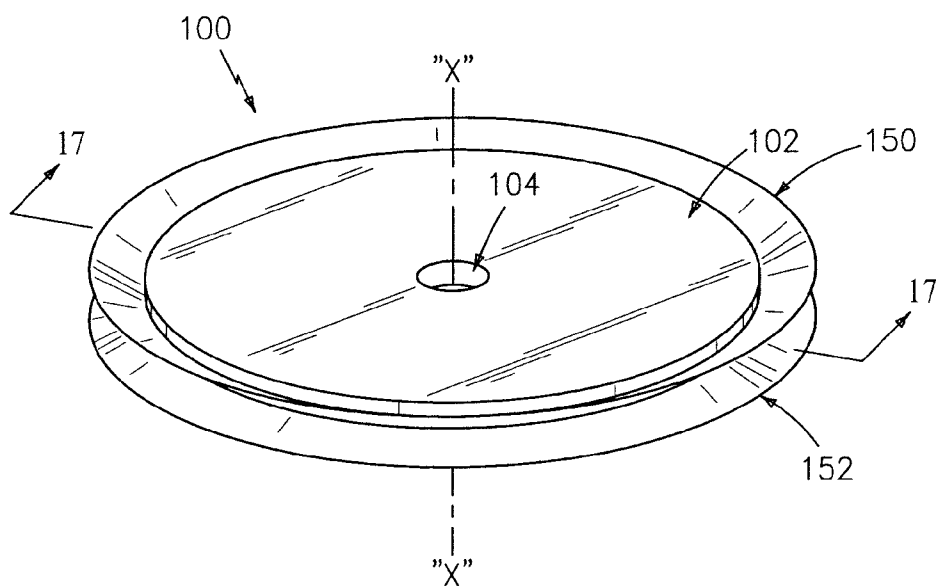


FIG. 16

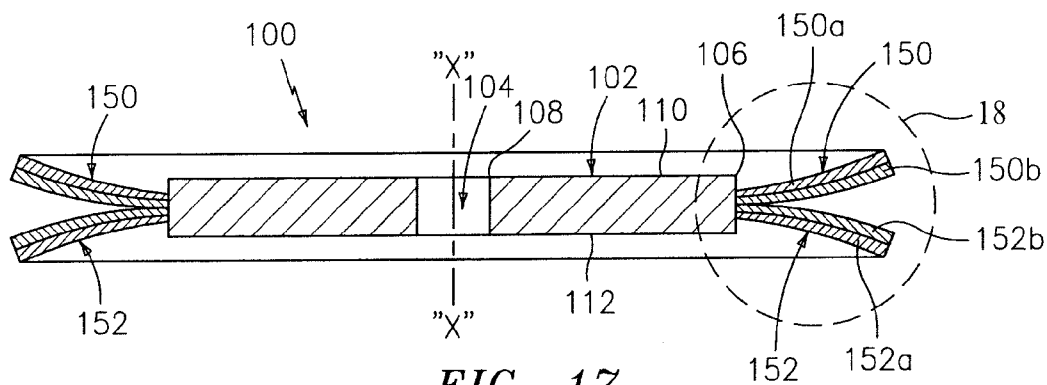


FIG. 17

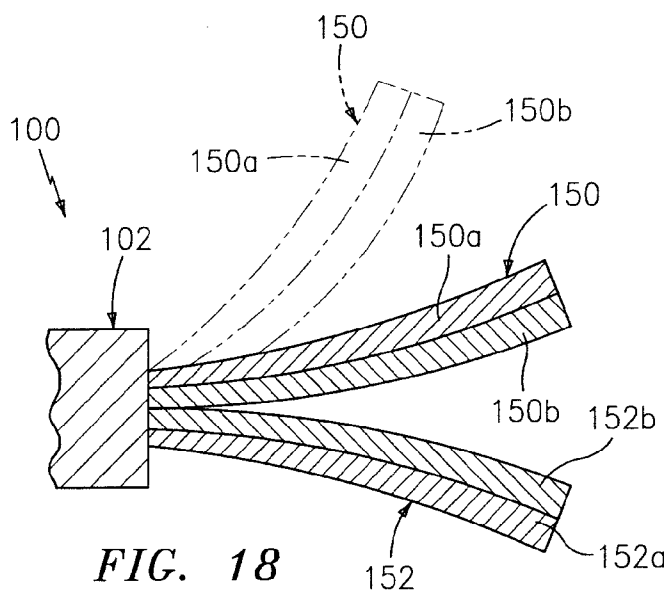


FIG. 18

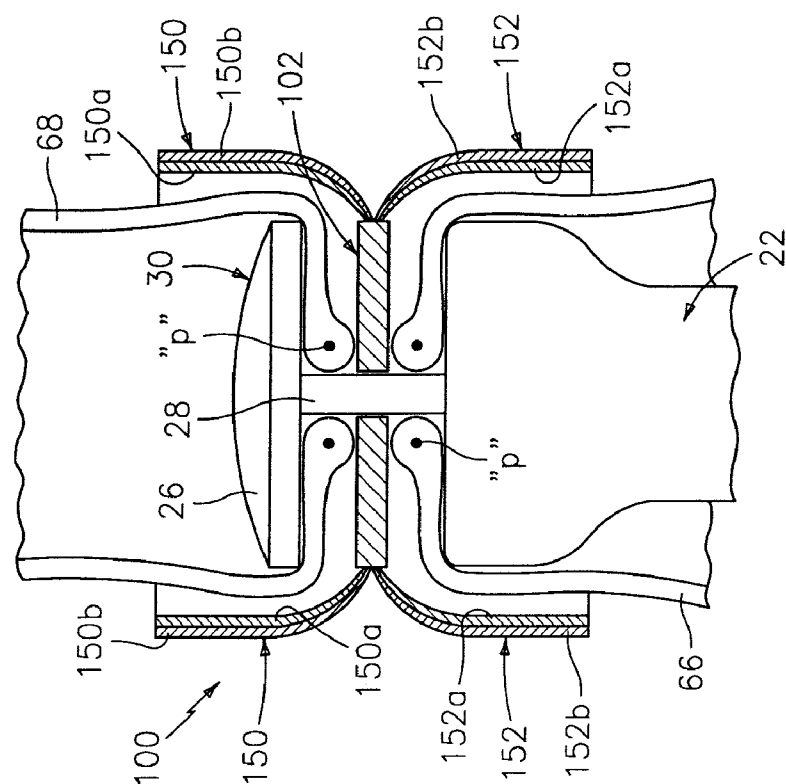


FIG. 19

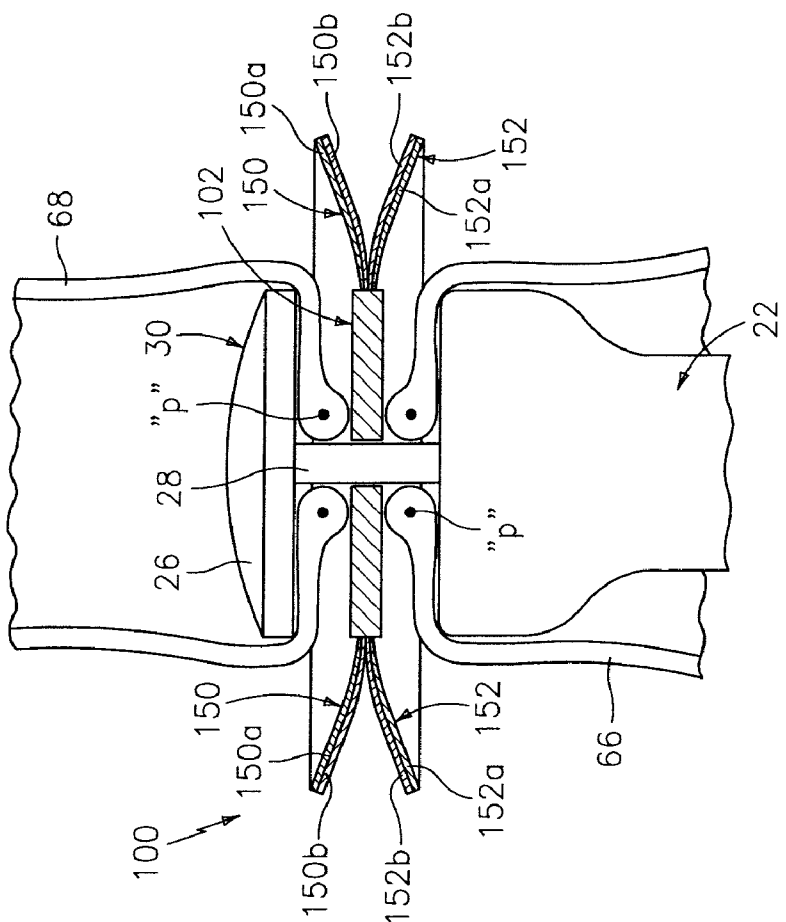
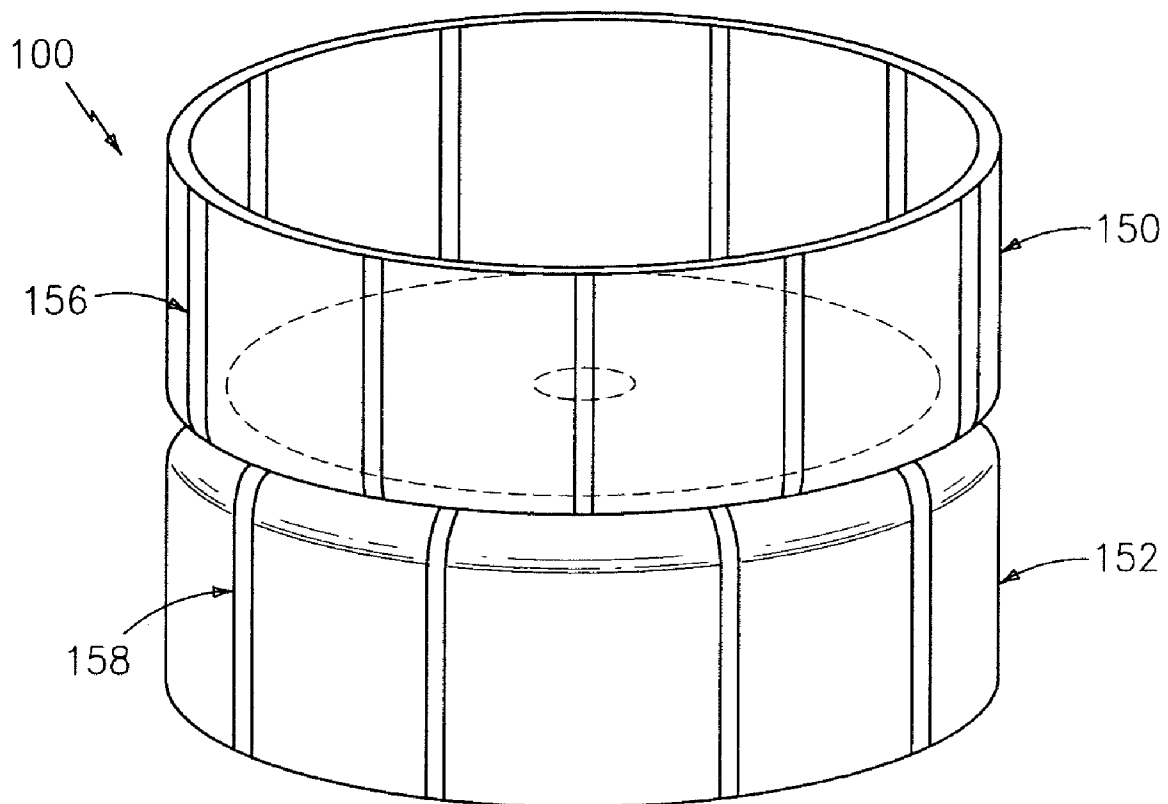


FIG. 20

*FIG. 21*

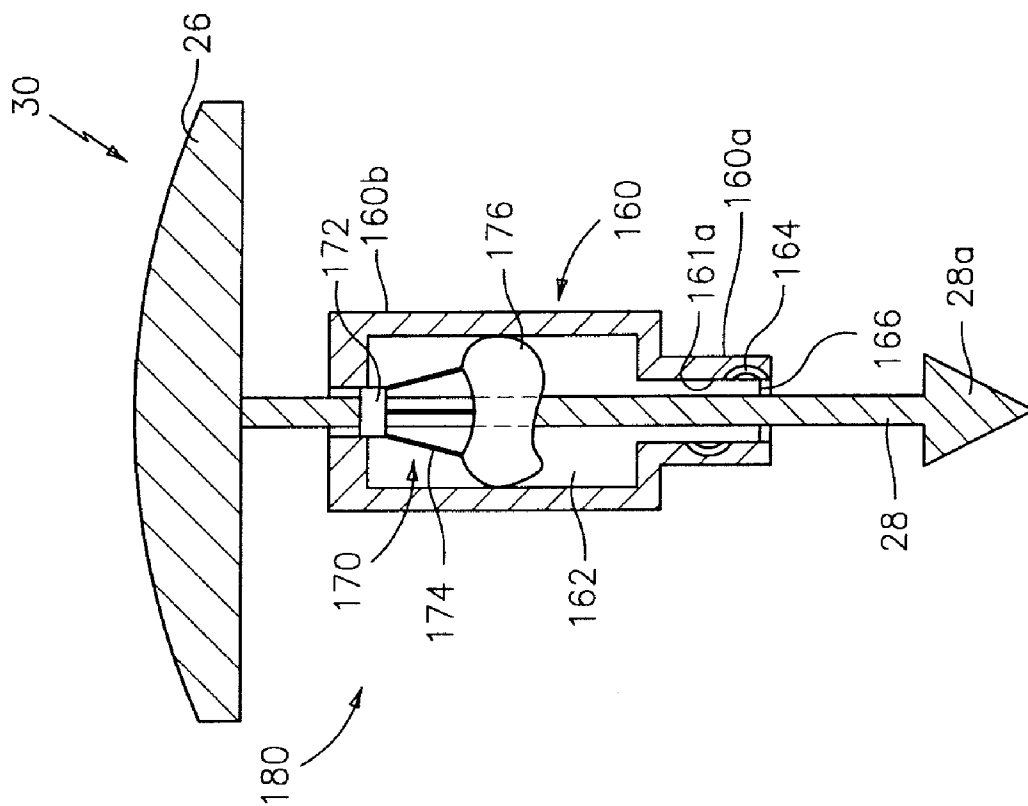


FIG. 23

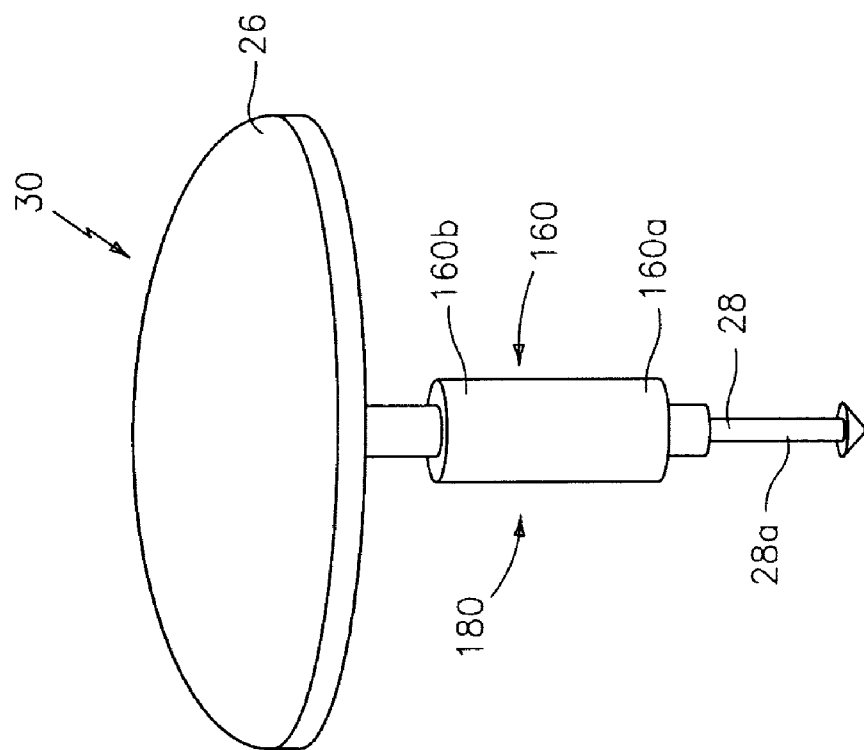


FIG. 22

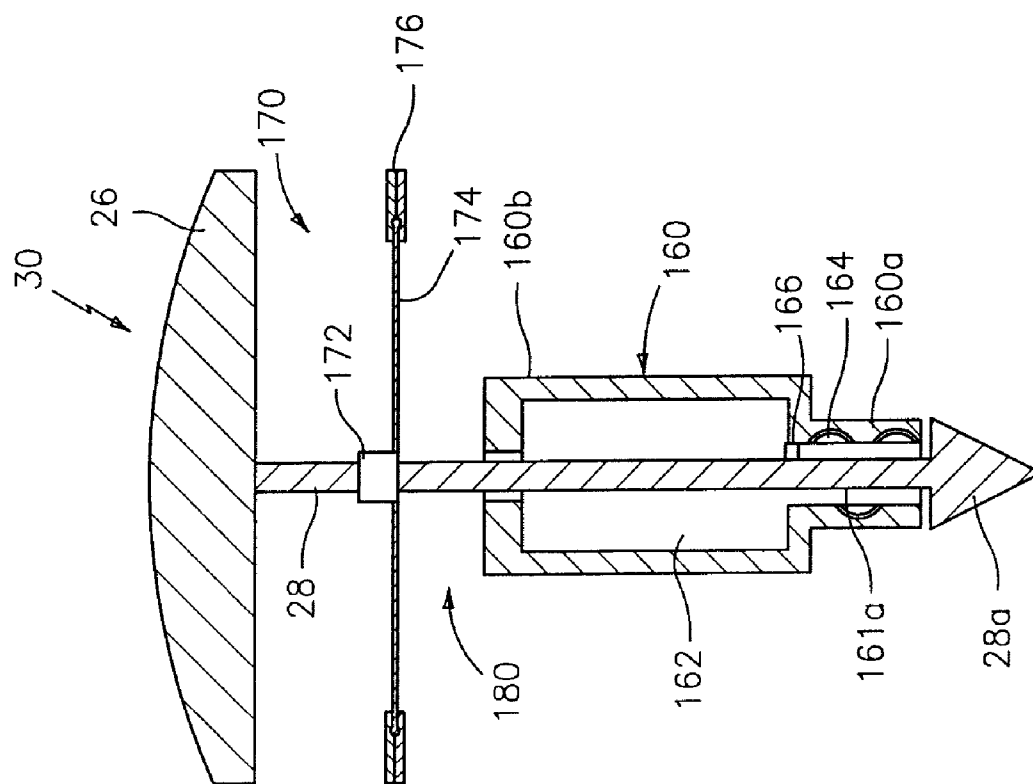


FIG. 25

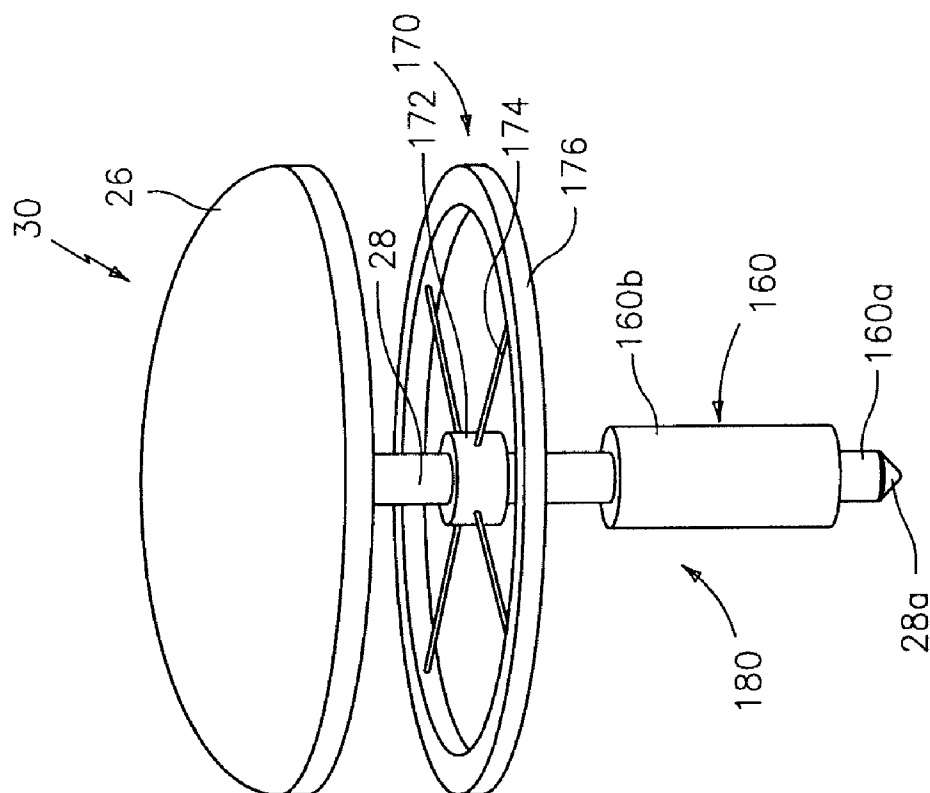


FIG. 24

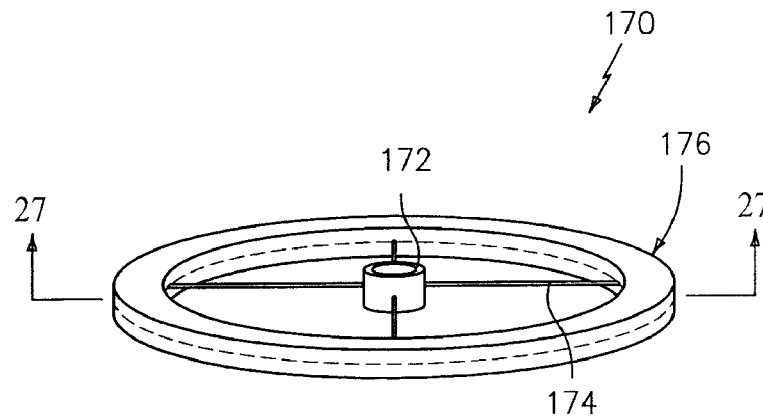


FIG. 26

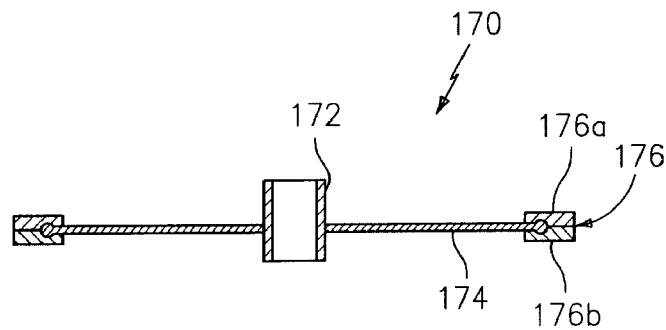


FIG. 27

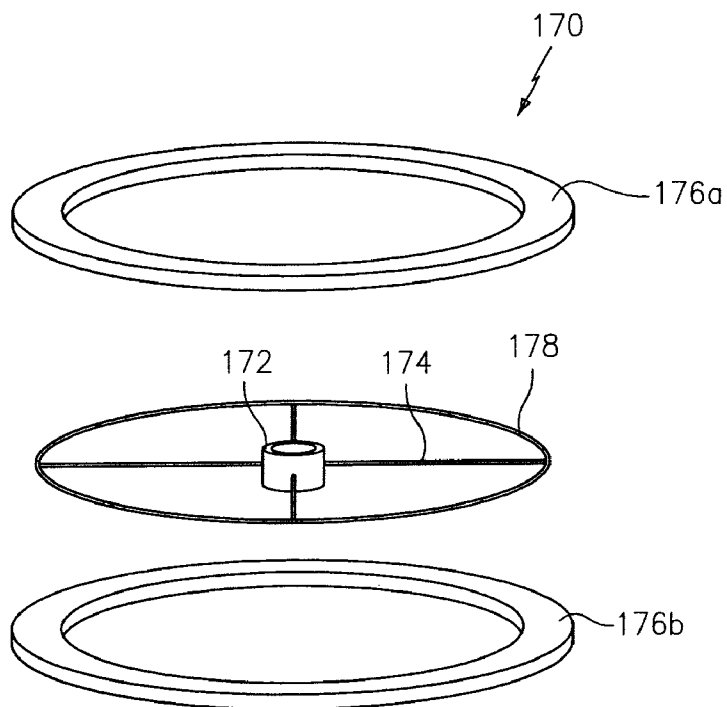


FIG. 28

FIG. 29

FIG. 30

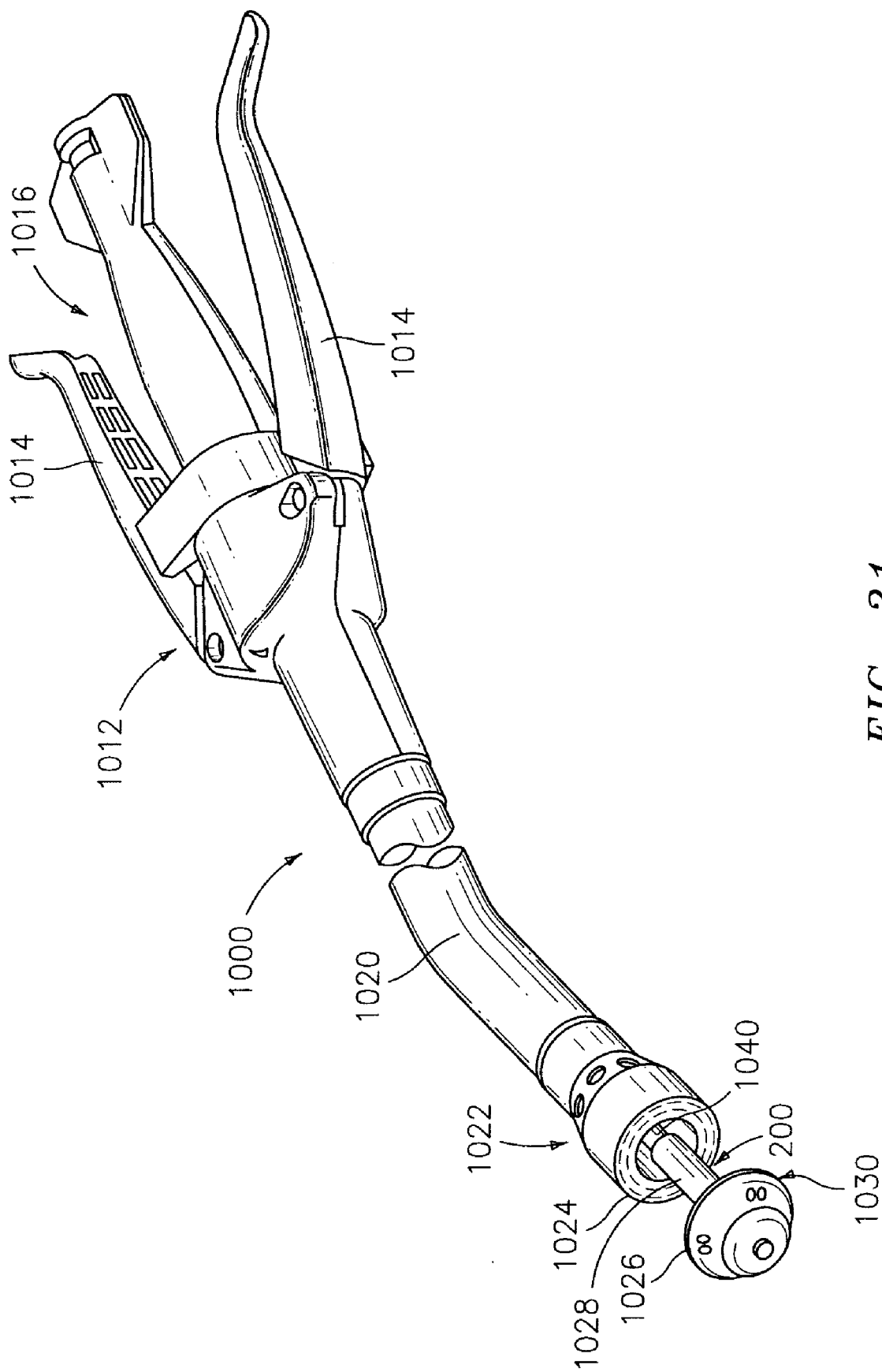


FIG. 31

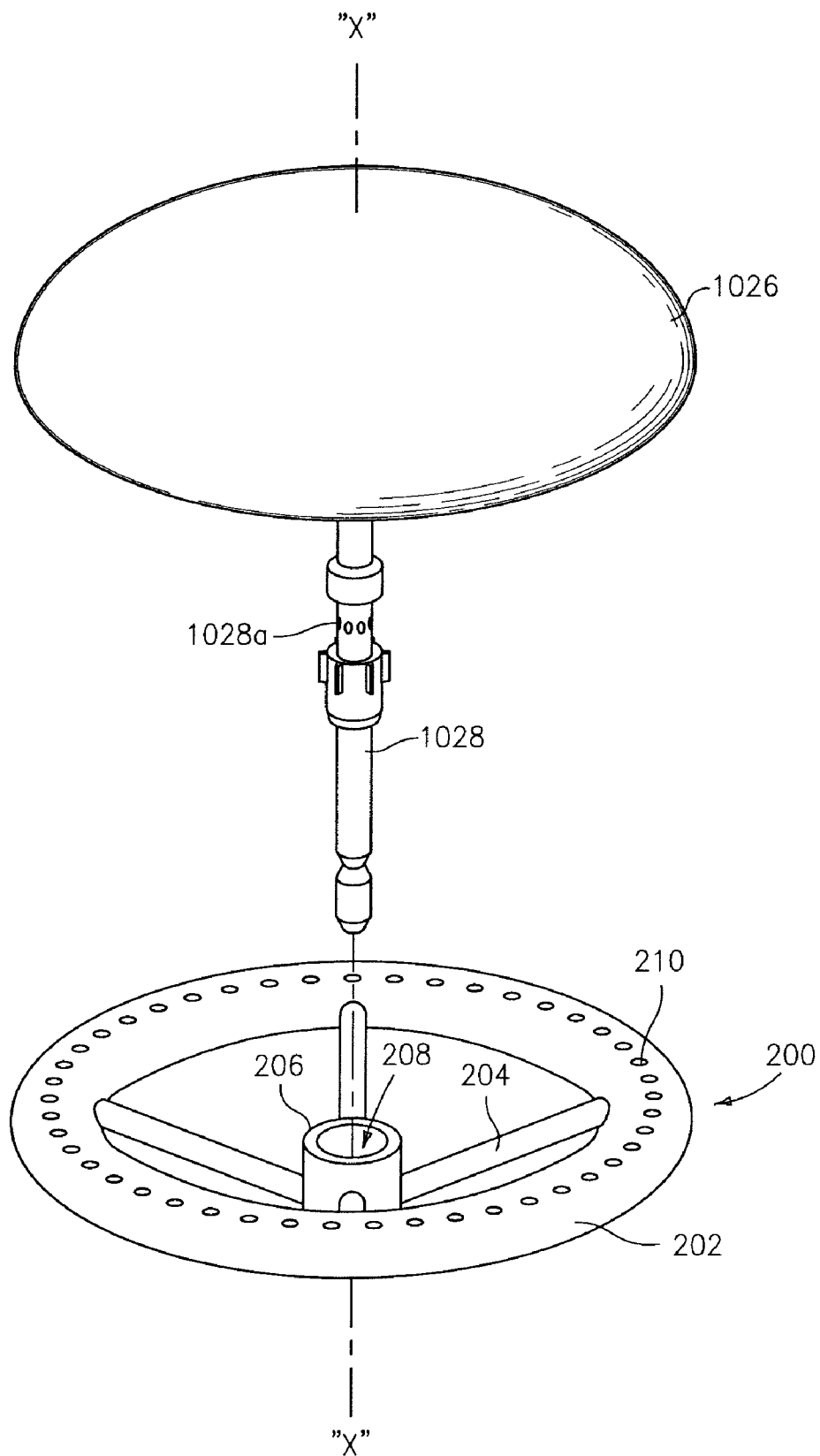


FIG. 32

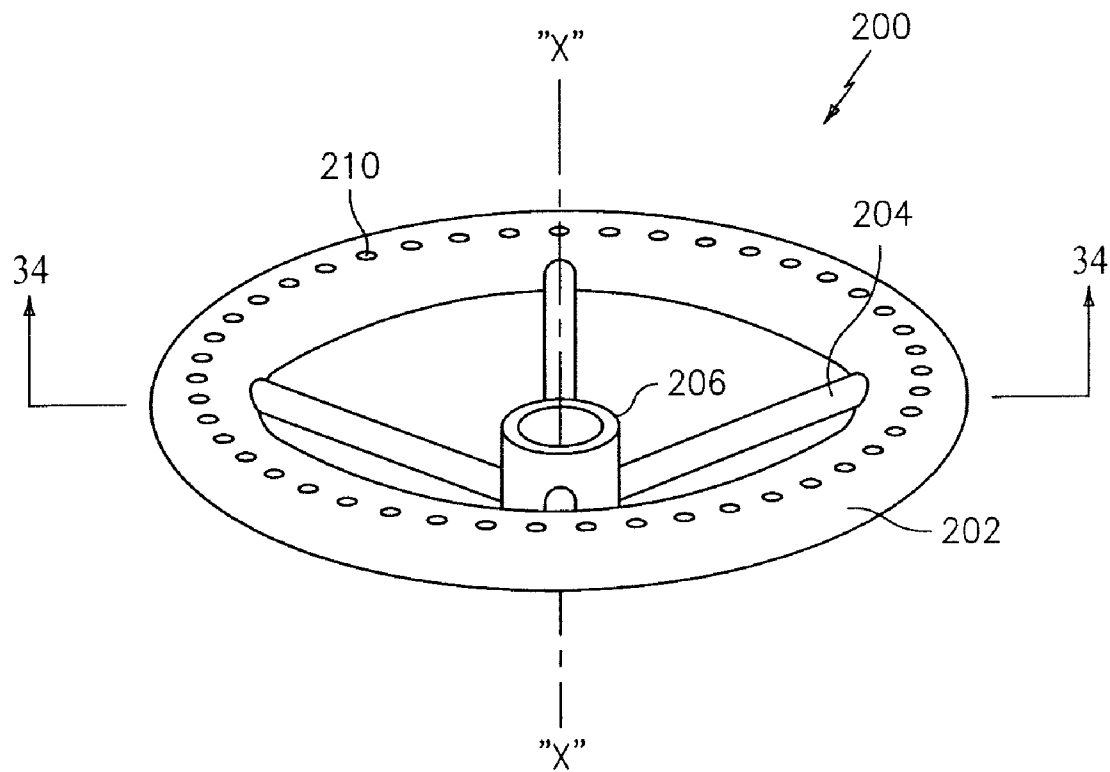


FIG. 33

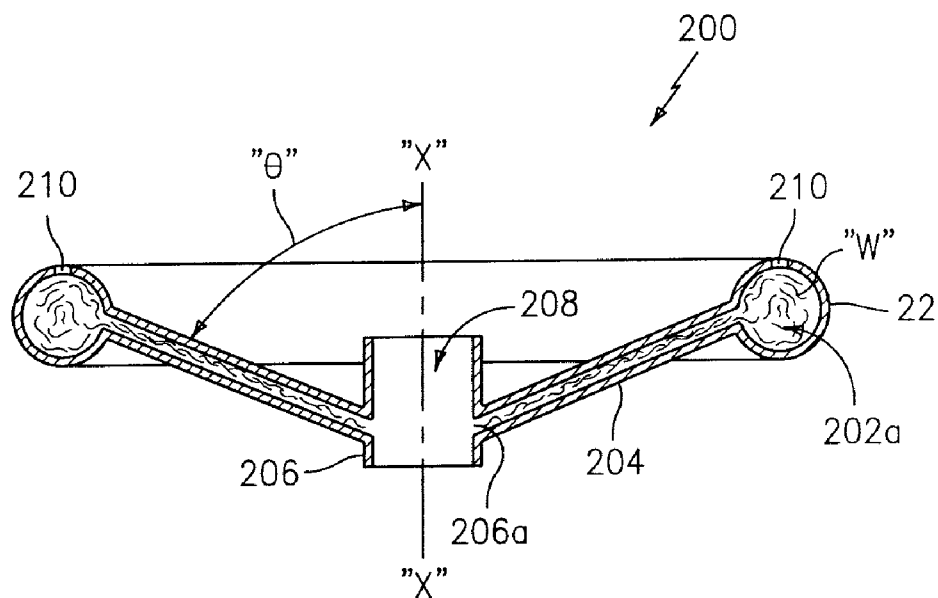


FIG. 34

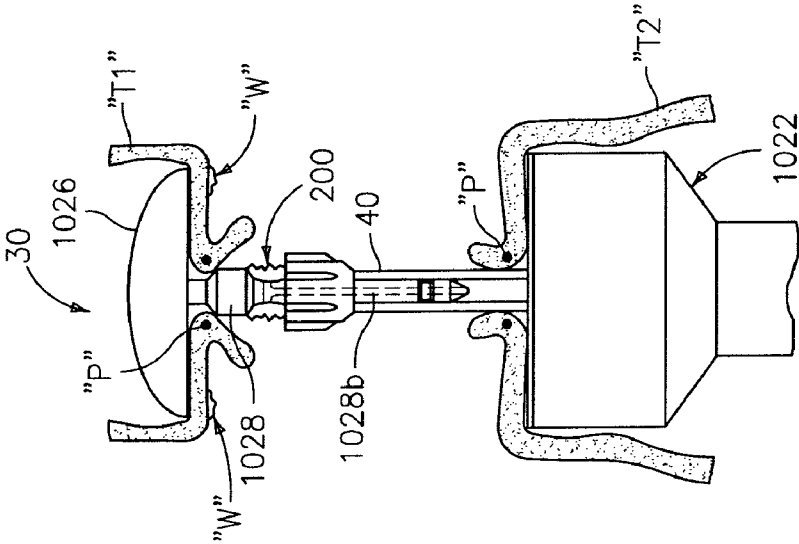


FIG. 35

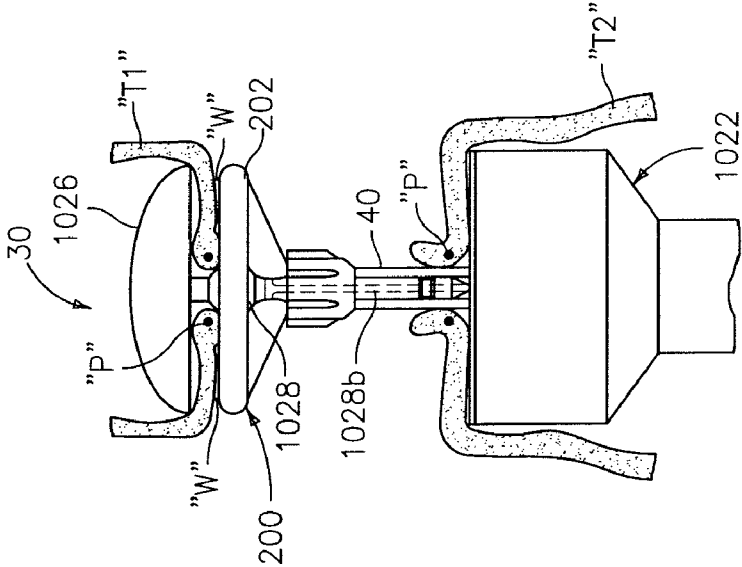


FIG. 36

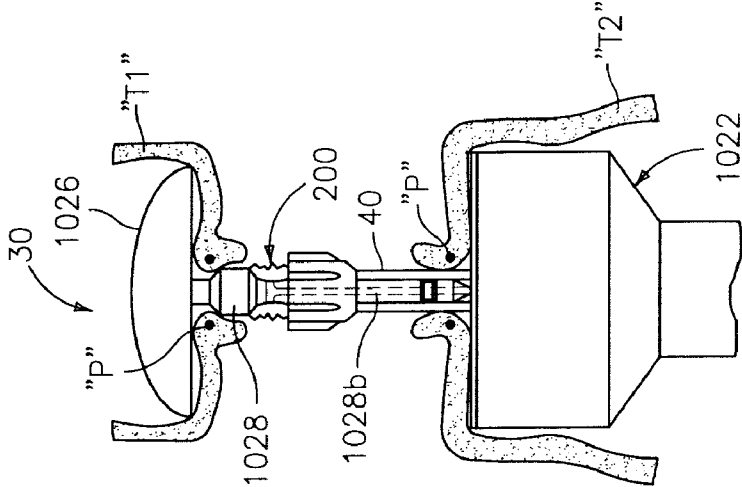


FIG. 37

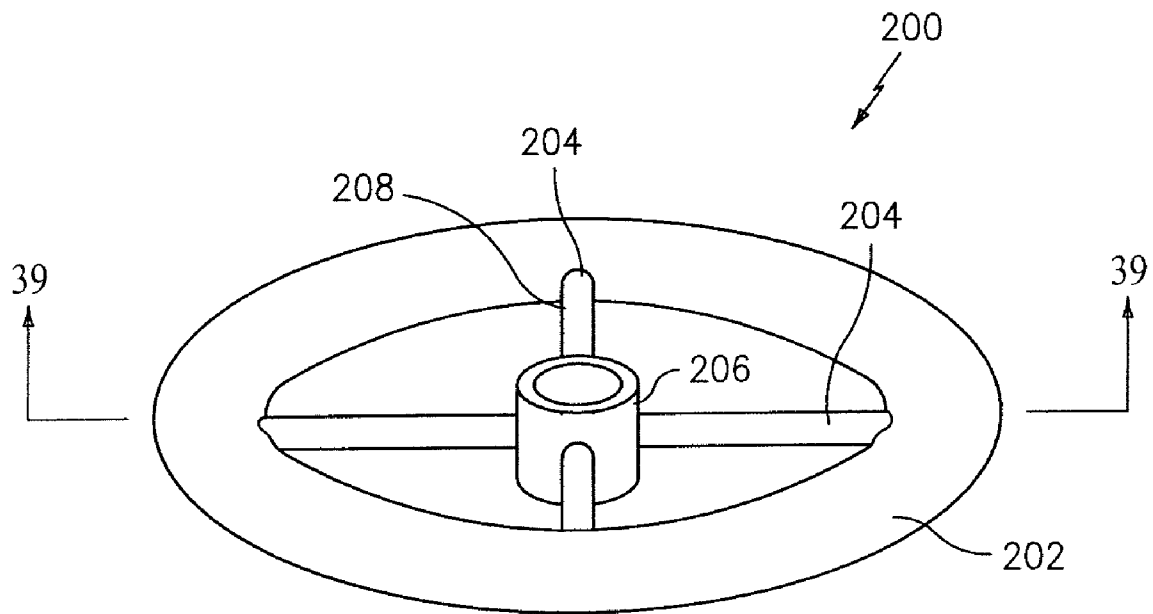


FIG. 38

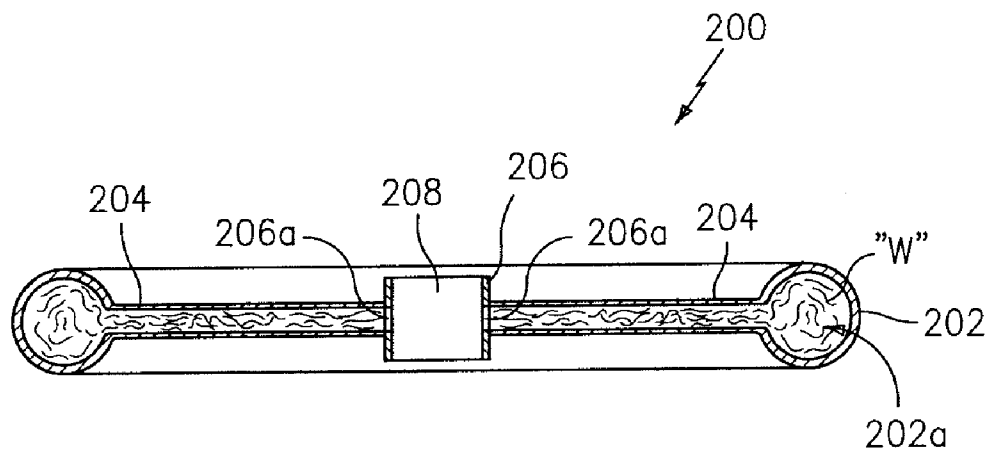


FIG. 39

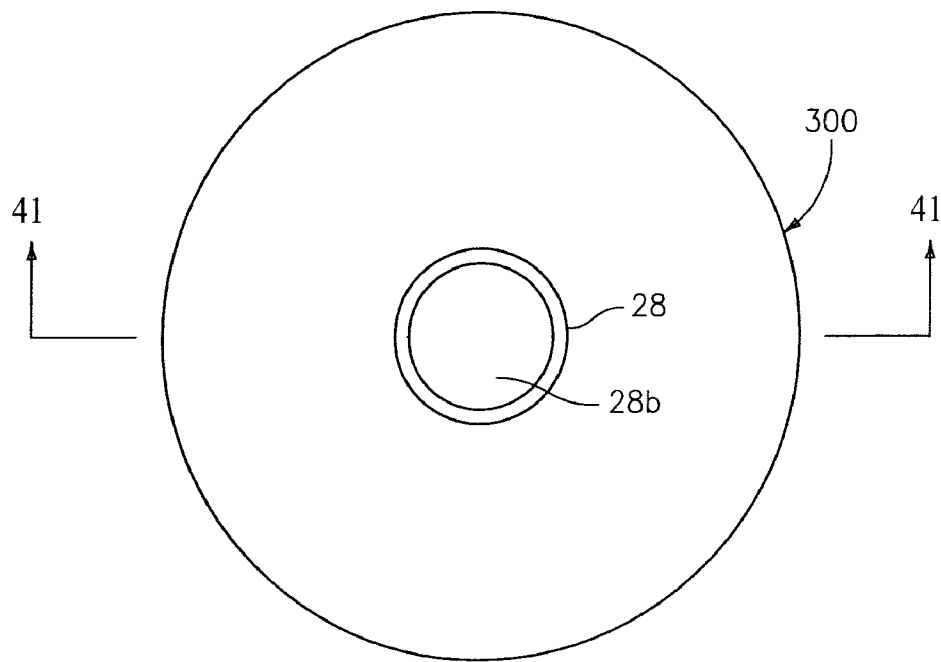


FIG. 40

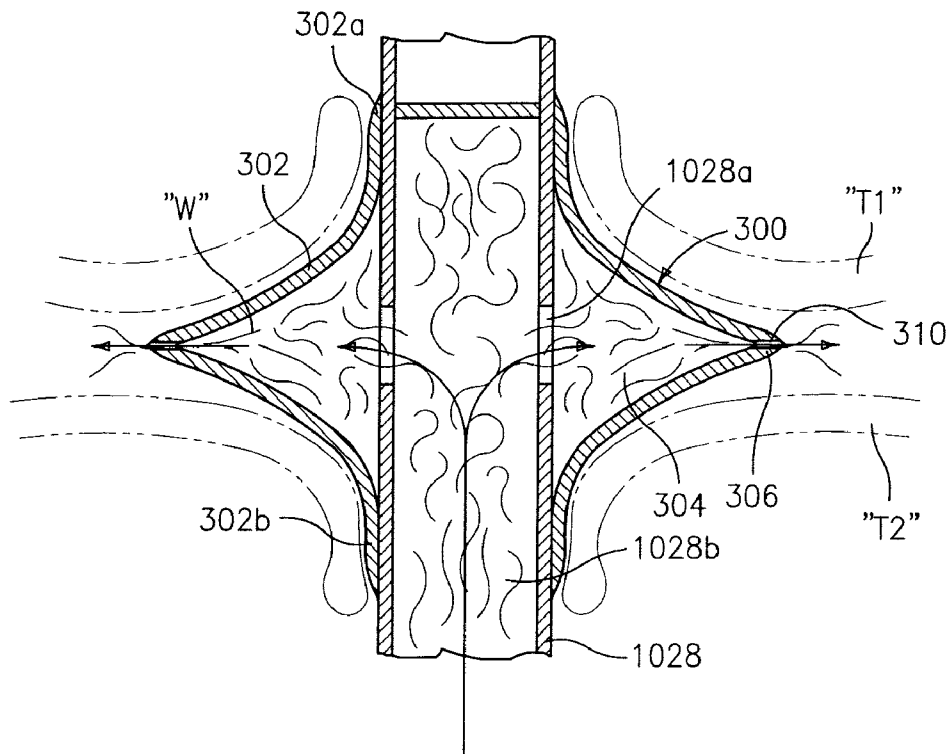


FIG. 41

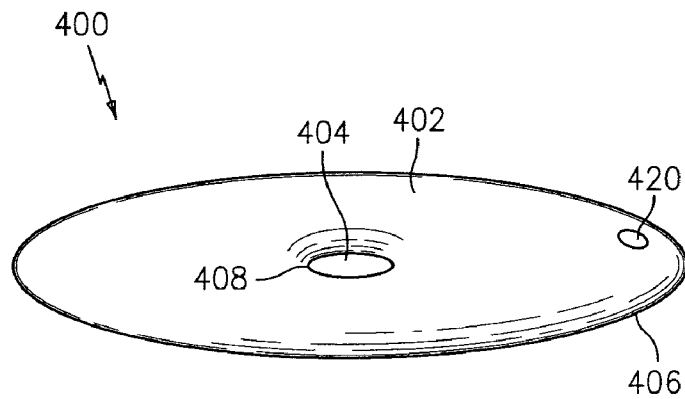


FIG. 42

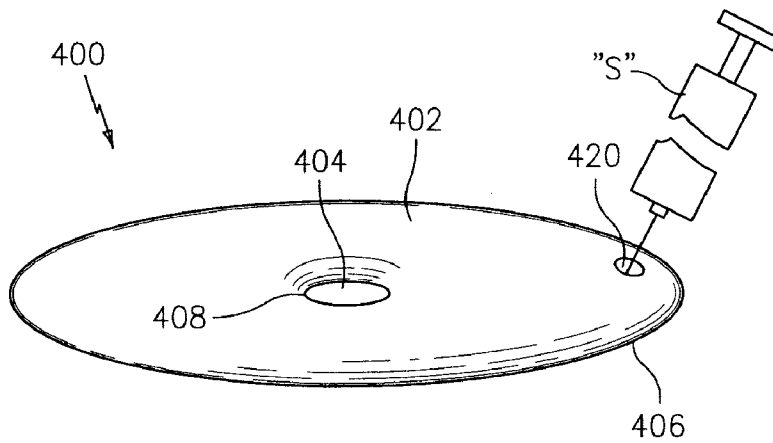


FIG. 43

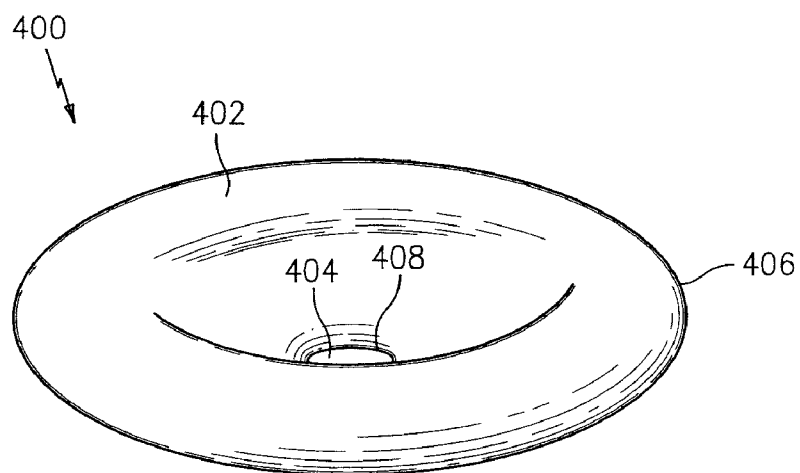


FIG. 44

ANNULAR ADHESIVE STRUCTURE

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a divisional of U.S. application Ser. No. 11/248,846 filed Oct. 12, 2005 now U.S. Pat. No. 7,823,592, which claims benefit of each of U.S. Provisional Application No. 60/620,268 filed Oct. 18, 2004, U.S. Provisional Application No. 60/620,269 filed Oct. 18, 2004, U.S. Provisional Application No. 60/620,066 filed Oct. 18, 2004, U.S. Provisional Application No. 60/620,140 filed Oct. 18, 2004 and U.S. Provisional Application No. 60/669,104 filed Apr. 7, 2005 and the disclosures of each of the above-identified applications are hereby incorporated by reference in their entirety.

BACKGROUND

1. Technical Field

The present disclosure relates to devices for applying structures and/or compositions including wound treatment materials, adhesives and/or sealing compositions, for use with or without stapling devices, for joining tissue, and for reducing occurrences of leaking, bleeding and/or stricture.

2. Background of Related Art

Throughout the years the medical field has utilized various techniques in an effort to join or bond body tissue together. Historically, suturing was the accepted technique for rejoining severed tissues and closing wounds. Suturing was achieved with a surgical needle and a suturing thread, and more recently, with a variety of polymeric or metallic staples, as will be discussed below. The intended function of sutures is to hold the edges of a wound or tissue against one another during the healing process so as to reduce discomfort, pain, scarring and the time required for healing.

Recently, many procedures which in the past required conventional suturing have been replaced by staple suturing which involves the application of the staples to the edges of the wound or tissue with the use of a surgical stapler. Surgical staplers have been developed for joining adjacent tissue, for providing hemostasis of adjacent tissue and for providing hemostasis in conjunction with cutting of adjacent tissue. Such surgical staplers include both linear and annular type configurations. A typical linear stapler and cutter includes parallel rows of staples with a slot for a cutting means to travel between the rows of staples.

Staples have traditionally been used to replace suturing when joining or anastomosing various body structures, such as, for example, the bowel or bronchus. The surgical stapling devices employed to apply these staples are generally designed to simultaneously cut and join an extended segment of tissue in a patient, thus vastly reducing the time and risks of such procedures.

Linear or annular surgical stapling devices are employed by surgeons to sequentially or simultaneously apply one or more rows of surgical fasteners, e.g., staples or two-part fasteners, to body tissue for the purpose of joining segments of body tissue together and/or for the creation of anastomoses. Linear surgical stapling devices generally include a pair of jaws or finger-like structures between which body tissue to be joined is placed. When the surgical stapling device is actuated and/or "fired", firing bars move longitudinally and contact staple drive members in one of the jaws, and surgical staples are pushed through the body tissue and into/against an anvil in the opposite jaw thereby crimping the staples closed. A knife blade may be provided to cut between the rows/lines of staples. Examples of such surgical stapling devices are

described in U.S. Pat. Nos. 4,354,628, 5,014,899 and 5,040,715, the entirety of each of which is incorporated herein by reference.

Annular surgical stapling devices generally include an annular staple cartridge assembly including a plurality of annular rows of staples, typically two, an anvil assembly operatively associated with the annular cartridge assembly, and an annular blade disposed internal of the rows of staples. Examples of such annular surgical stapling devices are described in U.S. Pat. Nos. 5,799,857 and 5,915,616 to Robertson et al., the entirety of each of which is incorporated herein by reference.

For most procedures, the use of bare staples, with the staples in direct contact with the patient's tissue, is generally acceptable. The integrity of the tissue will normally serve to prevent the staples from tearing out of the tissue and compromising the sealing before healing has occurred. However, in some surgical operations, surgical supports, e.g., meshes, are employed by surgeons to bridge, repair and/or reinforce tissue defects with a patient, especially those occurring in the abdominal wall, chest wall, diaphragm and other musculo-aponeurotic areas of the body. Examples of surgical supports are disclosed in U.S. Pat. Nos. 3,054,406, 3,124,136, 4,347,847, 4,655,221, 4,838,884 and 5,002,551, the entirety of each of which is incorporated herein by reference.

When the staples are applied in surgical procedures utilizing surgical meshes, supports, buttresses and the like (i.e., reinforcing material), the legs of the staple typically pass from the cartridge jaw through a layer of the surgical support, and through the patient's tissue before encountering the anvil jaw. In an alternative procedure, the legs of the staple typically pass from the cartridge jaw through a first layer of the surgical support, then through the patient's tissue, and finally through a second layer of the surgical support before encountering the anvil jaw. With the staples in place, the stapled tissue is clamped between the layers of the surgical support. Reference may be made to U.S. Pat. No. 5,542,594, the entire content of which is incorporated herein by reference, for a more detailed discussion of the use of surgical supports in cooperation with surgical stapling instrument.

In addition to the use of surgical staples, biological tissue adhesives have been developed for joining tissue. Generally, biological adhesives bond separated tissues together. Such adhesives may be used instead of suturing and stapling, for example, in surgical procedures, for the repair of tissue or the creation of anastomoses.

In addition to the use of biological adhesives, following the formation of the anastomosis, a separate instrument or device is used to apply biological sealants to the outer surface of the anastomosis. Typically, in a separate step, the biological sealants are applied to the outer surface of the anastomosis. The biological sealants are intended to reduce and/or stop the incidents of leakage from the anastomosis.

One possible side effect of any end-to-end bowel anastomosis is its tendency to stenosis over time, which stenosis can decrease the diameter of the lumen over time. Accordingly, the need exists for a surgical support structure which operates in conjunction with any end-to-end anastomosis device and assists in maintaining the lumen of the anastomosed bowel or other tubular organ open over time.

The application of suitable biocompatible adhesive offers many advantages to the patient and the surgeon alike, such as, for example, the possible reduction in the number of staples used, immediate sealing of the tissue being treated, a strengthening of the anastomosis, and a reduction in the occurrence of bleeding from the blood vessels, leakage

3

through the tissue joint, and stricture. Moreover, use of bio-compatible adhesives tends to minimize foreign body reaction and scarring.

There is a need for surgical stapling instruments and devices, which reduce the trauma suffered by a patient, reduce the number of gaps between or at individual staple sites, reduce leakage of fluids, reduce bleeding, and/or which create a relatively strong bond between adjacent body tissues, e.g., along staple lines and tissue seams.

Accordingly, the need exists for devices for applying structures and compositions which operate with or without surgical staples to assist in maintaining the joined tissue, including maintaining the tubular organs patent or open over time.

A need also exists for structures which operate with or without surgical staples to reduce the trauma suffered by the patient, reduce the instances of leakage, reduce the instances of bleeding, and create a relatively strong bond between adjacent body tissues.

SUMMARY

The present disclosure relates to support structures containing and/or capable of containing adhesive compositions therein, and which may be used in conjunction with stapling devices, for reducing occurrences of leaking, bleeding and/or stricture.

According to an aspect of the present disclosure, a method of joining tissue is provided. The method includes the steps of providing an apparatus having an anvil; and a body portion juxtaposed with respect to one another along a shaft and arranged so as to be approximated with respect to one another. The method further includes the steps of deploying a support structure from the shaft so as to dispose the support structure between a first tissue section and a second tissue section, the support structure including a wound treatment material for joining tissue; and approximating the anvil and body portion with one another so that the support structure is interposed between the first tissue section and the second tissue section.

The support structure may be bio-absorbable. The support structure may be a mesh-like material.

The support structure may be deployed from a first collapsed condition to a second expanded condition prior to the step of approximating.

The support structure includes a resilient material operatively associated therewith. The resilient material expands the support structure from the first collapsed condition to the second expanded condition, thereby deploying the support structure.

The support structure includes an inflatable tube. The tube is deployable from the first collapsed condition to the second expanded condition. The tube defines an interior space for receiving the wound treatment material therein in order to expand the support structure. The interior space of the tube defines a first chamber for receiving a first part of a two-part wound treatment material. The interior space of the tube defines a second chamber for receiving a second part of the two-part wound treatment material.

The body portion of the apparatus may have a plurality of staples for being deployed against the anvil. Each of the plurality of staples has a second part of the two-part wound treatment material.

The support structure may include a first layer and a second layer. The first layer of the support structure includes a first part of a two-part wound treatment material, and the second layer of the support structure includes a second part of the two-part wound treatment material.

4

The support structure includes a first part of a two-part wound treatment material. The method includes the step of applying a second part of the two-part wound treatment material to the support structure. The wound treatment material includes an adhesive material. The method further includes the step of puncturing the tube.

BRIEF DESCRIPTION OF DRAWINGS

The accompanying drawings, which are incorporated in and constitute a part of this specification, illustrate embodiments of the disclosure and, together with a general description of the disclosure given above and the detailed description of the embodiments given below, serve to explain the principles of the disclosure, wherein:

FIG. 1 is a perspective view of an exemplary annular surgical stapling device;

FIG. 2 is a perspective view of a support structure in accordance with an embodiment of the present disclosure, for use with the annular surgical stapling device of FIG. 1;

FIG. 3 is a cross-sectional view of a support structure in accordance with an alternate embodiment of the present disclosure, as taken through 3-3 of FIG. 2, for use with the annular surgical stapling device of FIG. 1;

FIG. 4 is a perspective view of a support structure in accordance with another embodiment of the present disclosure, for use with the annular surgical stapling device of FIG. 1;

FIG. 5 is a perspective view of a support structure in accordance with yet another embodiment of the present disclosure, for use with the annular surgical stapling device of FIG. 1;

FIG. 6 is an exploded perspective view of the support structure of FIG. 5;

FIG. 7 is a cross-sectional view of the support structure of FIGS. 5 and 6, as taken through 7-7 of FIG. 5;

FIG. 8 is a perspective view of the intestinal area of a patient, illustrating a method of positioning any of the support structures of FIGS. 2-7 on the anvil rod of the annular stapling device of FIG. 1;

FIG. 9 is a schematic perspective view of the intestinal area of FIG. 8, illustrating the anvil rod mounted to the annular stapling device and having any of the support structure of FIGS. 2-7 disposed therebetween;

FIG. 10 is a perspective view of a support structure, according to another embodiment of the present disclosure, shown in an undeployed condition;

FIG. 11 is a cross-sectional view of the support structure of FIG. 10, as taken through 11-11 of FIG. 10;

FIG. 12 is a perspective view of the support structure of FIGS. 10 and 11, shown in a deployed condition;

FIG. 13 is a cross-sectional view of the support structure of FIGS. 10-12;

FIG. 14 is a longitudinal cross-sectional view illustrating the anvil rod mounted to the annular stapling device within a surgical site and the support structure of FIGS. 10-13, in an undeployed condition, disposed between the apposed surfaces of the tissue;

FIG. 15 is a longitudinal cross-sectional view illustrating the anvil rod mounted to the annular stapling device within a surgical site and the support structure of FIGS. 10-13, in a deployed condition, disposed between the apposed surfaces of the tissue;

FIG. 16 is a perspective view of an support structure according to an alternate embodiment of the present disclosure;

FIG. 17 is a cross-sectional view of the support structure of FIG. 16, as taken through 17-17 of FIG. 16;

5

FIG. 18 is an enlarged view of the indicated area of detail of FIG. 17;

FIG. 19 is a longitudinal cross-sectional view illustrating the anvil rod mounted to the annular stapling device within a surgical site and the support structure of FIGS. 16-18, in an undeployed condition, disposed between the apposed surfaces of the tissue;

FIG. 20 is a longitudinal cross-sectional view illustrating the anvil rod mounted to the annular stapling device within a surgical site and the support structure of FIGS. 16-18, in a deployed condition, disposed between the apposed surfaces of the tissue;

FIG. 21 is a perspective view of a support structure according to yet another alternate embodiment of the present disclosure;

FIG. 22 is a perspective view of an anvil assembly including a support structure assembly, according to another embodiment of the present disclosure, shown in a first condition;

FIG. 23 is a longitudinal cross-sectional view of the support structure assembly of FIG. 22;

FIG. 24 is a perspective view of the support structure assembly of FIGS. 22 and 23, shown in a second condition;

FIG. 25 is a longitudinal cross-sectional view of the support structure of FIG. 24;

FIG. 26 is a perspective view of a support structure for use with the assembly of FIGS. 22-25;

FIG. 27 is a cross-sectional view of the support structure of FIG. 26, as taken through 27-27 of FIG. 26;

FIG. 28 is an exploded perspective view of the support structure of FIGS. 26 and 27;

FIG. 29 is a longitudinal cross-sectional view of a distal end of the surgical stapling apparatus while disposed in an operative site, illustrating the support structure of FIGS. 22-28, while in the first condition; and

FIG. 30 is a longitudinal cross-sectional view of a distal end of the surgical stapling apparatus while disposed in an operative site, illustrating the support structure of FIGS. 22-28, while in the second condition;

FIG. 31 illustrates a perspective view of a surgical stapling apparatus according to another embodiment of the present disclosure;

FIG. 32 is a perspective view, with parts separated, of the anvil member of the surgical stapling apparatus of FIG. 31 including a support structure, in accordance with the present disclosure;

FIG. 33 is a perspective view of the support structure of FIG. 32, illustrated in an expanded condition;

FIG. 34 is a cross-sectional view of the support structure of FIG. 33, as taken through 34-34 of FIG. 33;

FIG. 35 is a side elevational view of a distal end of the surgical stapling apparatus of FIG. 31, shown positioned in the operative site, illustrating the support structure of FIGS. 32-35 in a first or deflated condition;

FIG. 36 is a side elevational view of the distal end of the surgical stapling apparatus of FIG. 31, shown positioned in the operative site, illustrating the support structure of FIGS. 32-34 in a second or inflated condition in order to dispense wound treatment material onto the surface of the tissue to be anastomosed;

FIG. 37 is a side elevational view of the distal end of the surgical stapling apparatus of FIG. 31, shown positioned in the operative site, illustrating the wound treatment applying structure of FIGS. 32-34 in a third or deflated condition following dispensing of the wound treatment material onto the surface of the tissue to be anastomosed;

6

FIG. 38 is a perspective view of a support structure in accordance with another embodiment of the present disclosure, in an expanded condition, for use with the annular surgical stapling device of FIG. 31;

FIG. 39 is a cross-sectional view of the support structure of FIG. 38, as taken through 39-39 of FIG. 38;

FIG. 40 is a top plan view of a support structure in accordance with another embodiment of the present disclosure, shown in a deployed condition;

FIG. 41 is a cross-sectional view of the support structure of FIG. 40 as taken through 41-41 of FIG. 40;

FIG. 42 is a perspective view of a support structure, according to yet another embodiment of the present disclosure, shown in a collapsed or deflated condition;

FIG. 43 is a perspective view of the support structure of FIG. 42 being filled or inflated from a remote source of fluid; and

FIG. 44 is a perspective view of the support structure of FIGS. 42 and 43, shown in a filled or inflated condition.

DETAILED DESCRIPTION OF EMBODIMENTS

Embodiments of the presently disclosed devices and structures will now be described in detail with reference to the drawing figures wherein like reference numerals identify similar or identical elements. As used herein and as is traditional, the term "distal" refers to that portion which is furthest from the user while the term "proximal" refers to that portion which is closest to the user.

Referring initially to FIG. 1, an annular surgical stapling device, for use with the annular adhesive structures disclosed herein, is generally designated as 10. Surgical stapling device 10 includes a handle assembly 12 having at least one pivotable actuating handle member 14, and an advancing member 16. Extending from handle member 12, there is provided a tubular body portion 20 which may be constructed so as to have a curved shape along its length. Body portion 20 terminates in a staple cartridge assembly 22 which includes one or more arrays of staple receiving slots 36 having a staple (not shown) disposed in each one of staple receiving slots 36. Typically, a pair of annular arrays of staple receiving slots 36 is provided. Positioned distally of staple cartridge assembly 22 there is provided an anvil assembly 30 including an anvil member 26 and a shaft 28 operatively associated therewith for removably connecting anvil assembly 30 to a distal end portion or connection member 40 of stapling device 10.

Staple cartridge assembly 22 may be fixedly connected to the distal end of tubular body portion 20 or may be configured to concentrically fit within the distal end of tubular body portion 20. Typically, staple cartridge assembly 22 includes a staple pusher (not shown) including a proximal portion having a generally frusto-conical shape and a distal portion defining two concentric rings of peripherally spaced fingers (not shown), each one of which is received within a respective staple receiving slot 36.

Typically, a knife (not shown), substantially in the form of an open cup with the rim thereof defining a knife edge, is disposed within staple cartridge assembly 22 and mounted to a distal surface of the staple pusher (not shown). The knife edge is disposed radially inward of the pair of annular arrays of staples. Accordingly, in use, as the staple pusher is advanced, the knife is also advanced axially outward.

Reference may be made to U.S. Pat. No. 5,915,616 to Viola et al., the entire content of which is incorporated herein by reference, for a detailed discussion of annular stapling device 10. Although a circular stapling apparatus is shown in FIG. 1, the stapling device may be arranged to deploy staples in a

semi-circular or other desired shape. Although discussed with reference to intestinal tissue, devices according to the present disclosure can be arranged to join and/or treat other tissues in other procedures.

Turning now to FIG. 2, an adhesive or support structure, in accordance with an embodiment of the present disclosure, is generally designated as **100**. Structure **100** desirably has a shape corresponding to the arrays of staple receiving slots **36**. Preferably, the structure **100** includes a washer-like or disk-like body portion **102** including a substantially centrally located aperture **104** formed therethrough. Structure **100** is defined by an outer terminal edge **106**, an inner terminal edge **108** defining the size of aperture **104**, an upper surface **110**, and a bottom surface **112**.

In one embodiment, structure **100** is sized such that when structure **100** is operatively associated with stapling device **10**, as will be described in greater detail below, outer terminal edge **106** extends radially beyond staple retaining pockets **36** of staple cartridge assembly **22**. Additionally, aperture **104** of structure **100** is sized to at least receive shaft **28** of anvil assembly **30** therethrough. In another embodiment, the distance between outer terminal edge **106** and inner terminal edge **108** is substantially equal to a width of a tissue contact surface **24** (see FIG. 1) of staple cartridge assembly **22**.

It is contemplated that body portion **102** of structure **100** may be fabricated from or include a surgical grade, biocompatible, non-absorbable (i.e., permanent) material; desirably a mesh impregnated with an adhesive, sealant and/or wound treatment material. For example, body portion **102** may be fabricated from "TEFLON", which is a registered trademark owned by DuPont de Nemours & Co. It is further contemplated that body portion **102** may be fabricated from a biocompatible polymeric foam, felt, polytetrafluoroethylene (ePTFE), gelatin, fabric or the like, or any other biocompatible material.

Non-absorbable materials used for body portion **102** include, and are not limited to, those that are fabricated from such polymers as polyethylene, polypropylene, nylon, polyethylene terephthalate, polytetrafluoroethylene, polyvinylidene fluoride, and the like. Further non-absorbable materials include and are not limited to stainless steel, titanium and the like.

In one embodiment, body portion **102** of structure **100** may be fabricated from a bio-absorbable material which is desirably impregnated with an adhesive, sealant, and/or other wound treatment material (e.g., a medicament). Accordingly, a sealant component of structure **100** can be used to retard any bleeding which may occur from the tissue, an adhesive component of structure **100** can be used to secure the approximated tissue together, and the bio-absorbability of structure **100** allows for structure **100** to be absorbed into the body after a predetermined amount of time. For example, structure **100** may remain in place in the body for approximately 2-3 weeks in order for the anastomosis to sufficiently heal prior to structure **100** being absorbed into the body. In other embodiments, the structure **100** has at least one portion that is absorbable and at least one portion that is not absorbable.

Bio-absorbable materials used for body portion **102** of structure **100** include, and are not limited to, those fabricated from homopolymers, copolymers or blends obtained from one or more monomers selected from the group consisting of glycolide, glycolic acid, lactide, lactic acid, p-dioxanone, α -caprolactone and trimethylene carbonate. Other bio-absorbable materials include and are not limited to, for example, Polyglycolic Acid (PGA) and Polylactic Acid (PLA). In one

embodiment, body portion **102** may be fabricated from bio-absorbable felt, ePTFE, gelatin or any other bio-absorbable materials.

It is contemplated that the adhesive is a biocompatible adhesive including, but not limited to, adhesives which cure upon tissue contact, which cure upon exposure to ultraviolet (UV) light, which are two-part systems which are kept isolated from one another and cure upon coming into contact with one another, which are pressure sensitive, which are any combinations thereof, or any other known suitable adhesive. In one embodiment, it is contemplated that an adhesive having a cure time of from about 10 to 15 seconds may be used. In another embodiment, it is contemplated that an adhesive having a cure time of about 30 seconds may be used.

It is envisioned that body portion **102** of structure **100** may be impregnated with a pre-cured adhesive or sealant. The pre-cured sealant or adhesive will react with the moisture and/or heat of the body tissue to thereby activate the sealing and/or adhesive properties of the sealant or adhesive. It is envisioned that the pre-cured sealant or adhesive may be a hydro-gel or the like.

It is envisioned that the wound treatment material "W" includes and is not limited to one or a combination of adhesives, hemostats, sealants, coagulants, astringents, and medicaments. Other surgically biocompatible wound treatment materials "W" which may be employed in or applied by surgical instruments, including surgical staplers, include adhesives whose function is to attach or hold organs, tissues or structures; sealants to prevent fluid leakage; hemostats to halt or prevent bleeding; coagulants, astringents (e.g., sulfates of aluminum) and medicaments. Examples of adhesives which can be employed include protein derived, aldehyde-based adhesive materials, for example, the commercially available albumin/glutaraldehyde materials sold under the trade designation BioGlue™ by Cryolife, Inc., and cyanoacrylate-based materials sold under the trade designations Indermil™ and Derma Bond™ by Tyco Healthcare Group, LP and Ethicon Endosurgery, Inc., respectively. Examples of sealants, which can be employed, include fibrin sealants and collagen-based and synthetic polymer-based tissue sealants. Examples of commercially available sealants are synthetic polyethylene glycol-based, hydrogel materials sold under the trade designation CoSeal™ by Cohesion Technologies and Baxter International, Inc. Examples of hemostat materials, which can be employed, include fibrin-based, collagen-based, oxidized regenerated cellulose-based and gelatin-based topical hemostats. Examples of commercially available hemostat materials are fibrinogen-thrombin combination materials sold under the trade designations CoStasis™ by Tyco Healthcare Group, LP, and Tisseel™ sold by Baxter International, Inc.

The wound treatment material may include a cross-linking material and/or reactive agent that reacts with the support structure, tissue or both. The resulting material acts as a seal or tissue-joining material that is non-absorbable. For example, the wound treatment material may be based on biocompatible cross-linked polymers formed from water soluble precursors having electrophilic and nucleophilic groups capable of reacting and cross-linking in situ, including those disclosed in U.S. Pat. No. 6,566,406, the entire contents of which are incorporated herein by reference.

The wound treatment material may be disposed on structure **100** or impregnated into structure **100**. Medicaments may include one or more medically and/or surgically useful substances such as drugs, enzymes, growth factors, peptides,

proteins, dyes, diagnostic agents or hemostasis agents, monoclonal antibodies, or any other pharmaceutical used in the prevention of stenosis.

Wound treatment material "W" may include visco-elastic film forming materials, cross-linking reactive agents, and energy curable adhesives. It is envisioned that wound treatment material "W", and in particular, adhesive may be cured with the application of water and/or glycerin (e.g., 1,2,3-pranetetriol, also known as glycerol and glycerine) thereto. In this manner, the water and/or glycerin cure the adhesive and hydrate the wound.

In one embodiment, it is contemplated that body portion 102 of structure 100 may be impregnated with a first component of a two-part adhesive and that the device deploys the second component of the two-part adhesive. For example, in a surgical stapler 10, the staples, which are retained in staple receiving slots 36 of staple cartridge assembly 22, are coated with a second component (e.g., a reactant) of the two-part adhesive. In this manner, the first component of the adhesive is activated when the staples penetrate and capture body portion 102 of structure 100 during the firing sequence of surgical stapling device 10, and the two components of the adhesive contact one another.

As seen in FIG. 2, structure 100 may include a single layered body portion 102 including a homogeneous array of bio-absorbable or non-absorbable materials or a heterogeneous array of bio-absorbable and/or non-absorbable materials. In certain embodiments, body portion 102 is impregnated with a pressure sensitive adhesive which is activated when adjacent layers of tissue are approximated, with the body portion 102 disposed therebetween.

In an alternate embodiment, as seen in FIGS. 3 and 4, structure 100 may include a layered body portion having at least two layers as indicated by first layer, film or wafer 102a and second layer, film or wafer 102b. In this embodiment, each layer 102a, 102b may include a homogeneous or heterogeneous array of bio-absorbable and/or non-absorbable materials. It is envisioned that each layer 102a, 102b may be separated from one another, as seen in FIG. 4, prior to the surgical procedure.

As will be described in greater detail below, first layer 102a of structure 100 is placed against a surface of a first tissue to be anastomosed, in juxtaposition to a second tissue to be anastomosed, and second layer 102b of structure 100 is placed against a surface of the second tissue to be anastomosed, in juxtaposition to the first tissue to be anastomosed. In this manner, as the first and second tissues are brought into contact with one another first and second layers 102a, 102b of structure 100 are brought into contact with one another and allowed to mix and/or react. For example, first layer 102a of structure 100 includes a first component of a two-part adhesive or sealant while second layer 102b of structure 100 includes a second component of the two-part adhesive or sealant. Accordingly, in use, when first layer 102a and second layer 102b come into contact with one another, the first and second components of the two-part adhesive or sealant will also come into contact and mix to thereby form the adhesive or sealant.

First and second layers 102a, 102b may be fabricated as bio-absorbable film-like membranes which activate upon contact with one another and/or contact with a fluid (e.g., water, saline, blood, an activating fluid, etc.). It is envisioned that a break-way or tear-away divider or barrier (not shown) may be positioned between first and second layers 102a, 102b in order to prevent accidental and/or premature contact between first and second layers 102a, 102b. It is further envisioned that each first and second layer 102a, 102b may

include a liner (not shown) removably disposed on at least one of a top and bottom surface thereof. In any of these embodiments, prior to contact of first and second layers 102a, 102b with one another, the divider and/or liners must be removed in order for activation of the adhesive to occur.

It is further contemplated that the structure may be in the form of an absorbable gel pack filled with adhesive. For example, the structure may be a tubular ring, similar to annular adhesive structure 200 as will be described in greater detail below.

In accordance with an embodiment of the present disclosure, as seen in FIG. 4, it is envisioned that each layer 102a, 102b of structure 100 includes one portion of a hook and loop type fastener 120 (e.g., Velcro™). For example, first layer 102a includes a hook portion 120a of hook and loop type fastener 120 disposed on a surface thereof, and second layer 102b includes a loop portion 120b of the hook and loop type fastener 120 disposed on a surface thereof. Accordingly, in use, first and second layers 102a, 102b are secured to one another via the hook and loop type fastener so as to provide more time for the two components of the two-part adhesive or sealant to react with one another. Desirably, the hook and loop type fastener are fabricated from bio-absorbable materials.

As seen in FIGS. 5-7, each of first and second layers 102a, 102b of structure 100 includes an outer terminal edge 106a, 106b, respectively, and an inner terminal edge 108a, 108b respectively, defining a substantially centrally located aperture 104a, 104b, formed therethrough. Apertures 104a and 104b are axially aligned with one another and are sized to permit positioning of shaft 28 of anvil assembly 30 therethrough.

First and second layers 102a, 102b are sized such that when structure 100 is in an expanded condition, outer terminal edges 106a, 106b of first and second layers 102a, 102b extend radially beyond staple receiving slots 36 of staple cartridge assembly 22. First and second layers 102a, 102b may be fabricated from two laminated pieces of pliable material, such as, for example, ePTFE.

Structure 100 further includes a ring, hoop or other circular member 130 secured or disposed between first layer 102a and second layer 102b. Hoop 130 may be made from a resilient material, or a shape memory wire (e.g., NITINOL) wherein hoop 130 has a ring-like memorized shape.

It is envisioned that a layer of a reinforcing mesh or the like (not shown) may be disposed between first and second layers 102a, 102b, or incorporated within the first layer 102a and/or second layer 102b. In this manner, the reinforcing mesh may provide structure 100 with increased strength and structural integrity to maintain the patency of the lumen between the anastomosed tissues.

The inner terminal edge 108a, 108b of structure 100 is operatively connected to shaft 28 of anvil assembly 30, and the structure 100 is collapsed with hoop 130 biased against shaft 28 to thereby provide a low profile during insertion of anvil assembly 30 into the target surgical site. The structure 100 may be maintained collapsed against the shaft 28 by a breakable sleeve or removable member. In use, the anvil assembly 30 is connected to connection member 40 of tubular body portion 20 of surgical stapling device 10. Following insertion of anvil assembly 28, including structure 100, into the target surgical site and to the distal end of tubular body portion 20 of surgical stapling device 10, hoop 130 is allowed to return to its memorized shape thereby expanding structure 100 such that outer terminal edges 106a, 106b of first and second layers 102a, 102b extend radially beyond staple receiving slots 36 of staple cartridge assembly 22. The breakable sleeve may be broken upon introduction of wound treat-

11

ment material into the structure **100** or may be connected to an actuator at a proximal end of the device.

Since first and/or second layers **102a**, **102b** of structure **100** may be fabricated from a bio-absorbable material which is impregnated with a wound treatment material, such as an adhesive, a sealant, and/or a medicament, in use, the sealant component would function to retard any bleeding which may occur from the tissue, the adhesive component would function to secure the approximated tissue together, and the bio-absorbability of structure **100** allows for at least a portion of structure **100** to be absorbed into the body after a predetermined amount of time. It is envisioned that hoop **130** may be fabricated from a bio-absorbable material as well. In this manner, hoop **130** will ultimately be absorbed into the body. For example, in such an embodiment, structure **100** may be constructed such that first and second layers **102a**, **102b** remain in place in the body for approximately 2-3 weeks in order for the anastomosis to sufficiently heal while hoop **130** remains in place in the body for some time after that in order to help maintain the patency of the lumen.

Turning now to FIG. **8**, there is illustrated the use of surgical stapling device **10** and detachable anvil assembly **30** in an anastomosis procedure to effect joining of intestinal sections **66** and **68**. The anastomosis procedure is typically performed using minimally invasive surgical techniques including laparoscopic means and instrumentation. At the point in the procedure shown in FIG. **8**, a diseased intestinal section has been previously removed, anvil assembly **30** has been applied to the operative site either through a surgical incision or trans-anally and positioned within intestinal section **68**, and tubular body portion **20** of surgical stapling device **10** has been inserted trans-anally into intestinal section **66**. Intestinal sections **66** and **68** are also shown temporarily secured about their respective components (e.g., shaft **28** of anvil assembly **30**, and the distal end of tubular body portion **20**) by conventional means such as a purse string suture "P" (see FIG. **9**).

According to one method, as seen in FIG. **9**, if desired or if the surgical procedure requires, structure **100** may be placed onto shaft **28** of anvil assembly **30** prior to the coupling of anvil assembly **30** to the distal end of tubular body portion **20**. Following positioning of structure **100** onto shaft **28** of anvil assembly **30**, the surgeon maneuvers anvil assembly **30** until the proximal end of shaft **28** is inserted into the distal end of tubular body portion **20** of surgical stapling device **10**, wherein the mounting structure within the connection member **40** at the distal end of tubular body portion **20** engages shaft **28** to effect the mounting.

Thereafter, anvil assembly **30** and tubular body portion **20** are approximated using rotatable grip member **18** of handle member **12** to approximate intestinal sections **66**, **68** and capture structure **100** therebetween. Surgical stapling device **10** is then fired by manipulating the handle member **12** thereby stapling intestinal sections **66**, **68** to one another and cutting the portion of tissue and structure **100** disposed radially inward of the knife, to complete the anastomosis. Structure **100** may then release the adhesive impregnated therein to thereby adhere intestinal sections **66** and **68** to one another.

In the event that a structure **100**, having a first and second layer **102a**, **102b** each including one part of a two-part adhesive composition, is used, it is envisioned that first and second layers **102a**, **102b** are maintained separated and/or isolated from one another until approximation and firing of surgical stapling device is to occur. Accordingly, in use, one of first and second layers **102a**, **102b** may be placed on shaft **28** of anvil assembly **30**, against the surface of intestinal section **68**, while the other of first and second layers **102a**, **102b** is placed against the surface of intestinal section **66**. It is envisioned

12

that pins (not shown) may extend distally from the distal end of tubular body portion **20** and penetrate through intestinal section **66**. In this manner, the other of first and second layers **102a**, **102b** may be pinned onto the pins extending through intestinal section **66**.

Alternatively, if a structure **100**, having a first and second layer **102a**, **102b** each including one part of a two-part adhesive composition, is used, it is envisioned that each layer **102a**, **102b** may be provided with a tear-away or removable liner for maintaining first and second layers **102a**, **102b** separated and/or isolated from one another. Accordingly, both first and second layers **102a**, **102b** may be placed on shaft **28** of anvil assembly **30**.

If a structure **100**, having a first and second layer **102a**, **102b**, each including one part of a two-part adhesive composition, is used, the adhesive composition is activated upon first and second layers **102a**, **102b** coming into contact with one another.

Turning now to FIGS. **10-15**, in an embodiment of a support structure, support structure **100** includes at least one, preferably a pair of drapes, skirts or membranes **140**, **142** (e.g., a first membrane **140** and a second membrane **142**) extending from outer terminal edge **106** of body portion **102**. Desirably, membranes **140**, **142** are fabricated from a polymeric or plastic film including, and not limited to, polyethylene and the like. Each membrane **140**, **142** includes a first or outer surface **140a**, **142a**, respectively, and a second or inner surface **140b**, **142b**, respectively.

As seen in FIGS. **10** and **11**, membranes **140**, **142** have a first, undeployed condition wherein membranes **140**, **142** are rolled-up or others collapsed towards body portion **102**. Desirably, membranes **140**, **142** are rolled under in a direction toward the first or outer surfaces **140a**, **142a** thereof, as indicated by arrows "A" of FIG. **11**. As seen in FIGS. **12** and **13**, membranes **140**, **142** have a second, deployed condition wherein membranes **140**, **142** are unrolled or unfurled to extend in a substantially parallel orientation with respect to the central "X" axis. As will be described in greater detail below, first membrane **140** is unrolled in a first direction, preferably in a distal direction (e.g., in a direction extending away from upper surface **110** of body portion **102**), and second membrane **142** is unrolled in a second direction, preferably in a proximal direction (e.g., in a direction extending away from lower surface **112** of body portion **102**).

As seen in FIGS. **10** and **11**, support structure **100** desirably includes one or more rip-cords or tethers **144**, **146** rolled-up into membranes **140**, **142**. Rip-cords **144**, **146** include free ends **144a**, **146a** which extend from membranes **140**, **142** when membranes **140**, **142** are in the rolled-up condition. In this manner, as will be described in greater detail below, as rip-cords **144**, **146** are pulled, desirably in a distal direction and a proximal direction, membranes **140**, **142** are un-rolled or un-furled accordingly.

In one embodiment, it is envisioned that body portion **102** of support structure **100** is formed of a foam material overmolded onto a relatively thin flexible material or film integral with membranes or sleeves **140**, **142**. Desirably, when unrolled or un-furled, each membrane **140**, **142** extends approximately 2.0 cm from body portion **102**. In other words, when un-rolled or un-furled, first membrane **140** extends from body portion **102** by approximately 2.0 cm from upper surface **110** of body portion **102**, and second membrane **142** extends from body portion **102** approximately 2.0 cm from lower surface **112** of body portion **102**.

Turning now to FIGS. **14** and **15**, there is illustrated the use of surgical stapling device **10** and support structure **100** in an anastomosis procedure to effect joining of intestinal sections

13

66 and 68. The anastomosis procedure is typically performed using minimally invasive surgical techniques including laparoscopic means and instrumentation. At the point in the procedure shown in FIGS. 14 and 15, a diseased intestinal section has been previously removed, anvil assembly 30 has been introduced to the operative site either through a surgical incision or trans-anally and positioned within intestinal section 68, and tubular body portion 20 of surgical stapling device 10 has been inserted trans-anally into intestinal section 66. Intestinal sections 66 and 68 are also shown temporarily secured about their respective components (e.g., shaft 28 of anvil assembly 30, and the distal end of tubular body portion 20) by conventional means such as a purse string suture "P".

Support structure 100 is then placed onto shaft 28 of anvil assembly 30 prior to the coupling of anvil assembly 30 to the distal end of tubular body portion 20. In particular, shaft 28 of anvil assembly 30 is inserted into aperture 104 of body portion 102. Following positioning of structure 100 onto shaft 28 of anvil assembly 30, the surgeon maneuvers anvil assembly 30 until the proximal end of shaft 28 is inserted into the connection member 40 at the distal end of tubular body portion 20 of surgical stapling device 10, wherein the mounting structure (not shown) within the connection member 40 engages shaft 28 to effect the mounting.

Thereafter, as seen in FIG. 15, anvil assembly 30 and tubular body portion 20 are approximated to approximate intestinal sections 66, 68 and capture body portion 102 of structure 100 therebetween. With body portion 102 captured between intestinal sections 66, 68, as seen in FIG. 15, membranes 140, 142 are deployed (i.e., un-rolled or un-furled) as described above. In particular, first membrane 140 is un-rolled or un-furled in a distal direction, as indicated by arrow "B", so as to over-lie intestinal section 68, and second membrane 142 is un-rolled or un-furled in a proximal direction, as indicated by arrow "C", so as to over-lie intestinal section 66. Desirably, first and second membranes 140, 142 are un-rolled or un-furled by pulling on rip-cords 144, 146 in a distal or proximal direction, as necessary.

Membranes 140, 142 extend a predetermined distance over intestinal sections 66 and 68 (e.g., approximately 2 cm). When un-rolled or un-furled, membranes 140, 142 desirably adhere to the surface of intestinal sections 66, 68. The membranes may comprise a pressure-sensitive adhesive, or other adhesive material, incorporated with the membranes or coated thereon. Membranes 140 and 142 function to inhibit leakage from the anastomosis site and/or function to strengthen or reinforce intestinal sections 66, 68. With membranes 140, 142 deployed, as seen in FIG. 15, surgical stapling device 10 may be fired thereby stapling intestinal sections 66, 68 to one another and cutting the portion of tissue and structure 100 disposed radially inward of the knife, to complete the anastomosis.

Turning now to FIGS. 16-21, structure 100 includes at least one, preferably a pair of membranes 150, 152 (e.g., a first membrane 150 and a second membrane 152) extending from outer edge 106 of body portion 102. Each membrane 150 and 152 includes two layers, an inner layer 150a, 152a, respectively, and an outer layer 150b, 152b, respectively. Desirably, the materials selected for the construction of membranes 150, 152 swell at different rates when in the presence of moisture or fluid. In this manner, membranes 150, 152 will tend to bend or curl about the layer having the relatively slower rate of fluid swelling or fluid absorption. In this manner, support structure 100 has a first undeployed condition in which membranes 150, 152 extend substantially radially outward from body

14

portion 102, and a second deployed condition in which membranes 150, 152 are substantially aligned with the central "X" axis of body portion 102.

In accordance with one embodiment, it is envisioned that inner layer 150a, 152a of membranes 150, 152 are constructed from a material that does not substantially absorb moisture or non-expanding (i.e., static) material, such as, for example, a bio-absorbable mesh fabricated from polyglycolic acid, sold under the tradename Dexon™, available from Tyco Healthcare Group L.P., Norwalk, Conn. It is also envisioned that outer layer 150b, 152b of membranes 150, 152 are constructed from a moisture absorbing or expanding (i.e., dynamic) material, such as, for example, hydrogel and the like.

Desirably, each membrane 150 and 152 includes a hydrogel outer layer 150b, 152b laminated to a bio-absorbable mesh inner layer 150a, 152a. Furthermore, support structure 100 includes a foam body portion 102 laminated over the layered membrane 150, 152 materials. While each membrane 150, 152 desirably includes a pair of layers, it is envisioned and within the scope of the present disclosure for membranes 150, 152 to include any number of layers.

Accordingly, with reference to FIG. 18, the difference in material properties between inner layers 150a, 152a and outer layers 150b, 152b of membranes 150, 152 cause membranes 150, 152 to curl or bend from the undeployed condition, wherein membranes 150, 152 extend in a substantially radial direction, to a deployed condition, wherein membranes 150, 152 extend in a direction substantially parallel to the central "X" axis (as shown in phantom in FIG. 18).

Turning now to FIGS. 19 and 20, there is illustrated the use of surgical stapling device 10 and support structure 100 including membranes 150, 152 in an anastomosis procedure to effect joining of intestinal sections 66 and 68. At the point in the procedure shown in FIG. 19, anvil assembly 30 and tubular body portion 20 are shown approximated to one another to capture body portion 102 of annular support structure 100 between intestinal sections 66 and 68, wherein intestinal section 66 and 68 were previously secured about their respective components (e.g., shaft 28 of anvil assembly 30, and the distal end of tubular body portion 20) by conventional means such as a purse string suture "P", annular support structure 100 was positioned between intestinal sections 66 and 68, and anvil assembly 30 was coupled to the distal end of tubular body portion 20.

With body portion 102 of support structure 100 captured between intestinal sections 66, 68, as seen in FIGS. 12 and 13, membranes 150, 152 begin to deploy (i.e., curl or bend from the substantially radially extended orientation to the orientation substantially parallel with the central "X" axis) as described above. In particular, as outer layers 150b, 152b of first and second membranes 150, 152 absorb fluid and swell (i.e., expand), first and second membranes 150, 152 curl or bend to the side of membrane 150, 152 which swells or expands at a rate slower, i.e., toward inner layers 150a, 152a. As membranes 150, 152 are deployed, as indicated by arrow "B", first membrane 150 over-lies intestinal section 68, and second membrane 152 over-lies intestinal section 66, as indicated by arrow "C".

Desirably, membranes 150, 152 extend a predetermined distance over intestinal sections 66 and 68 (e.g., approximately 2 cm). Membranes 150, 152 are arranged so that they will adhere to the surface of intestinal sections 66, 68. Membranes 150, 152 function to inhibit leakage from the anastomosis site and/or function to strengthen or reinforce intestinal sections 66, 68. With membranes 150, 152 deployed, as seen in FIG. 20, surgical stapling device 10 may be fired thereby

15

stapling intestinal sections **66**, **68** to one another and cutting the portion of tissue and structure **100** disposed radially inward of the knife, to complete the anastomosis.

In a further embodiment, as seen in FIG. **21**, structure **100** includes a series of ribs **156**, **158** provided on and/or in each membrane **150**, **152**, respectively. Desirably, ribs **156**, **158** are spaced radially around the perimeter or circumference of membranes **150**, **152**. Ribs **156**, **158** are substantially axially oriented.

Ribs **156**, **158** are fabricated from a shape memory material, alloy or the like, preferably, NITINOL™ and the like. Alternatively, the ribs may be fabricated from a polymeric material. It is further envisioned that ribs **156**, **158** may be fabricated from a bio-absorbable or non-absorbable material.

Ribs **156**, **158** have a memorized shape which is oriented substantially parallel to the central “X” axis of support structure **100**. In this manner, support structure **100** has a first or un-deployed condition in which ribs **156**, **158** are in a biased rolled-up or otherwise collapsed condition and membranes **150**, **152** are also rolled-up or otherwise collapsed, and a second or deployed condition in which ribs **156**, **158** are in their memorized shape or unbiased condition and membranes **150**, **152** are extended.

In use, with support structure in an un-deployed condition, support structure **100** is positioned on shaft **28** of anvil assembly **30**. With support structure **100** so positioned, support structure **100** is deployed when ribs **156**, **158** return to their memorized conditions. In particular, the return of ribs **156**, **158** to their memorized conditions extends membranes **150**, **152** over intestinal sections **66** and **68** and/or in a direction substantially parallel to the central “X” axis.

Turning now to FIGS. **22-30**, a support structure assembly, in accordance with an embodiment of the present disclosure, is generally designated as **180** and is operatively supported on shaft **28** of anvil assembly **30**. As mentioned above, anvil assembly **30** includes an anvil member **26** and a shaft **28**, extending from anvil member **26** and being operatively connectable with a distal end portion of stapling device **10**.

Anvil assembly **30** includes a support structure assembly **180** operatively disposed on shaft **28** thereof. Support structure assembly **180** includes sleeve **160** operatively disposed on shaft **28** of anvil assembly **30**. Sleeve **160** includes a proximal portion **1610a** having a diameter slightly larger than the diameter of shaft **28**, and a distal portion **160b** having a diameter larger than the diameter of proximal portion **160a** and defining a chamber **162** between shaft **28** and distal portion **160b**.

Sleeve **160** is movable along the length of shaft **28** from a first position in which sleeve **160** is in close proximity to anvil member **30** (see FIGS. **22** and **23**) and a second position in which sleeve **160** is spaced a distance from anvil member **28** (see FIGS. **24** and **25**). Desirably, a cam surface **164** is formed in an inner surface **161a** of proximal portion **160a** of sleeve **160**. Additionally, a cam follower **166** is provided on shaft **28** and operatively engages cam surface **164** of sleeve **160**. Desirably, during use, anvil **26** is drawn closer to the tubular body portion **20**, as discussed above. The cam follower **166** rides in cam surface **164** so that sleeve **160** is axially displaced with respect to shaft **28** (e.g., between the first and second positions). Preferably, as shaft **28** is drawn proximally, the cam follower **166** and cam surface **164** interact so that sleeve **160** moves proximally move quickly than shaft **28**.

Support structure assembly **180** further includes a support structure **170** operatively supported on shaft **28**. Support structure **170** has a collapsed or first condition, as seen in FIG. **23**, wherein support structure **170** is retained within chamber **162** of sleeve **160**, and an expanded or second condition, as

16

seen in FIGS. **24** and **25**, wherein support structure **170** is free from chamber **162** of sleeve **160** and extends radially outward from shaft **28**.

As seen in FIGS. **23-28**, and in particular FIGS. **26-28**, support structure **170** preferably includes a central hub **172**, a plurality of spokes **174** extending from hub **172**, and a disc **176** operatively connected to the distal end of spokes **174**. Desirably, support structure **170** includes a ring **178** operatively connected to the distal end of each spoke **174**. Ring **178** and spokes are desirably resilient and collapsible and provides disc **176** with an increased degree of structural integrity. Preferably, spokes **174** and ring **178** are made from a wire of shape memory material (e.g., NITINOL and the like), wherein spokes **174** and/or ring **178** have a memorized shape with the spokes radially oriented with respect to hub **172** and ring **178** having a hoop-like shape.

As best seen in FIGS. **27** and **28**, disc **176** preferably includes a first disc **176a** disposed on a first side of ring **178**, and a second disc **176b** disposed on a second side of ring **178**. Preferably, discs **176a**, **176b** have a width sufficient to extend across staple receiving slots **36**. In this manner, as will be discussed in greater detail below, when surgical stapling device **10** is fired, staples **38** (see FIGS. **29** and **30**) are driven through discs **176a**, **176b**.

It is contemplated that first and second discs **176a**, **176b** may be fabricated from any of the materials disclosed above. In an embodiment, first and second discs **176a**, **176b** are impregnated with a wound treatment material.

Turning now to FIGS. **29** and **30**, a method of using support structure assembly **180** is shown and described. The anastomosis procedure is typically performed using minimally invasive surgical techniques including laparoscopic means and instrumentation. At the point in the procedure shown in FIG. **29**, a diseased intestinal section has been previously removed, anvil assembly **30** has been applied to the operative site, and distal end **22** of body portion **20** (i.e., the tubular body portion) of surgical stapling apparatus **10** has been inserted into a second intestinal section **68**.

According to the present method, following positioning of anvil assembly **30** and the distal end of tubular body portion **20** within intestinal sections **66** and **68**, respectively, the surgeon maneuvers anvil assembly **30** until a proximal end of shaft **28** is inserted into a connection member **40** provided in the distal end of tubular body portion **20** of surgical stapling device **10**. Connection member **40** desirably connects the proximal end of shaft **28** and proximal portion **160a** of sleeve **160** in order to effect the mounting of anvil assembly **30** to tubular body portion **20**. Connection member **40** may include a rod **41** disposed within the tubular body portion **20** which has a detent structure for engaging shaft **28**.

Thereafter, anvil assembly **30** and tubular body portion **20** are approximated to approximate intestinal sections **66**, **68** and move sleeve **160** from the first position to the second position in order to deploy support structure **170**. In particular, during approximation of anvil assembly **30** and tubular body portion **20**, as seen in FIG. **29**, sleeve **160** is moved in a proximal direction, from the first position to the second position (as indicated by arrow “A”), relative to shaft **28**, as discussed above.

As sleeve **160** is moved in a proximal direction relative to shaft **28**, support structure **170** is exposed from a distal end of sleeve **160**. As seen in FIG. **30**, once sleeve **160** has moved in the proximal direction relative to shaft **28** by an amount sufficient for the distal end thereof to completely clear support structure **170** or until proximal portion **160a** of sleeve **160** abuts against, e.g., bottoms out against, an enlarged head **28a** provided at a proximal end of shaft **28**, support structure

17

170 is deployed (i.e., spokes 174 and ring 178 are returned to their memorized or pre-biased conditions).

As seen in FIG. 30, with support structure 170 deployed, disc 176 is expanded between first and second intestinal sections 66, 68 and substantially overlies and/or comes into registration with staple receiving slots 36 of staple cartridge assembly 22. With support structure 170 deployed between first and second intestinal sections 66, 68, anvil assembly 30 is further approximated toward tubular body portion 20 to thereby clamp disc 176 between first and second intestinal sections 66, 68. With anvil assembly 30 fully approximated toward body portion 20, surgical stapling device 10 is fired thereby stapling disc 176 between intestinal sections 66, 68. Additionally, concomitantly therewith, the knife (not shown) is actuated to sever the portion of intestinal sections 66, 68 and the portion of spokes 174 located radially inward from the knife, thereby completing the anastomosis.

From the foregoing, it will be appreciated that disc 176 of support structure 170 functions to strengthen the anastomosis and reduce the occurrence of bleeding, leaking and stricture. It is also to be appreciated that the annular adhesive structures of the present disclosure may be utilized in a number of other applications and is not limited solely to bowel or bronchus anastomosis.

Turning now to FIGS. 31-37, a support structure 200, in accordance with an alternate embodiment of the present disclosure, is shown supported on stem 1028 of anvil member 1026 of annular surgical stapling device 1000. Surgical stapling device 1000 is substantially similar to surgical stapling device 10 and will only be discussed in detail to the extent necessary to identify differences in construction and operation.

As seen in FIGS. 32-34, support structure 200 includes an outer circular rim, tube or doughnut 202, a plurality of spokes 204 extending radially inward from circular tube 202, and a central hub 206 operatively joining spokes 204. Circular tube 202 is generally toroidal in shape when in an expanded condition. Central hub 206 defines a lumen 208 therethrough, having a central longitudinal "X" axis, for receipt of stem 1028 of anvil member 1026.

As seen in FIG. 34, circular tube 202 of support structure 200 defines a cavity 202a therein, and spokes 204 act as conduits for transmitting fluid (e.g., wound treatment material "W") to cavity 202a of circular tube 202. Central hub 206 includes a plurality of apertures 206a formed therein and which are in fluid communication with spokes 204. Apertures 206a of central hub 206 are in fluid communication with ports 1028a (see FIG. 32) formed in stem 1028 of anvil member 1026. Ports 1028a are in fluid communication with a conduit or passage 1028b extending axially through stem 1028 of anvil member 1026. Conduit 1028b is fluidly connected to a source of fluid (not shown), when anvil member 1026 is coupled to connection means 1040 (see FIG. 31), in order to deliver a fluid (e.g., wound treatment material "W") to cavity 202a of circular tube 202.

Support structure 200 has a first unexpanded or deflated condition in which cavity 202a of circular tube 202 is unfilled and circular tube 202 and spokes 204 are wrapped around, collapsed onto, or otherwise in close proximity to stem 1028 of anvil member 1026. Support structure 200 has an expanded condition in which cavity 202a of circular tube 202 is filled with wound treatment material "W".

As seen in FIGS. 32-34, circular tube 202 is provided with a plurality of perforations 210 formed therein. Preferably, perforations 210 are formed along an upper or distal surface 203 of circular tube 202. Additionally, perforations 210 extend at least partially around, and preferably completely

18

around, the circumference or perimeter of circular tube 202. In this manner, as will be described in greater detail below, wound treatment material "W" is dispensed from perforations 210 when circular tube 202 is expanded or inflated with wound treatment material "W".

As seen in FIG. 34, spokes 204 are angled by a degree "Θ" with respect to the longitudinal "X" axis of hub 206. Desirably, spokes 204 are angled in a distal direction when support structure 200 is in an inflated condition. In one embodiment, when support structure 200 is in the inflated condition, spokes 204 are angled by a degree "Θ" and sufficient for circular tube 202 to be in close proximity to a tissue contacting surface of anvil member 1026. Preferably, as will be described in greater detail below, when support structure 200 is in the inflated condition, circular tube 202 will substantially contact the tissue "T" purse string sutured to anvil member 1026.

While support structure 200 has been shown and described as including hub 206, it is envisioned and within the scope of the present disclosure that spokes 204 may be directly connected to stem 1028 and, more particularly, fluidly connected to ports 1028a of stem 1028.

It is envisioned that the wound treatment material "W" can include one or a combination of wound treatment materials, such as adhesives, hemostats, sealants, medicaments and the like as described above.

Turning now to FIGS. 35-37, a method of using support structure 200 for distributing and/or dispensing wound treatment material is shown and described. The anastomosis procedure is typically performed using minimally invasive surgical techniques including laparoscopic means and instrumentation. At the point in the procedure shown in FIG. 35, a diseased intestinal section has been previously removed, anvil assembly 1030 has been applied to the operative site, and distal end 1022 of body portion 1020 (i.e., the tubular body portion) of surgical stapling apparatus 1000 has been inserted into a second intestinal section "T2".

Following positioning of anvil assembly 1030 and distal end 1022 of body portion 1020 within intestinal sections "T1 and T2", the surgeon maneuvers anvil assembly 1030 until the proximal end of stem 1028 is inserted into the distal end of connection means 1040 to effect mounting of anvil assembly 1030 to connection means 1040. With anvil assembly 1030 mounted to connection means 1040, as seen in FIG. 35, support structure 200 is expanded to the inflated condition by injecting wound treatment material "W", through conduit 1028b of stem 1028, through spokes 204, and into cavity 202a of circular tube 202. The proximal end of the tubular body portion desirably includes a button, plunger or other actuator for dispensing wound treatment material to support structure 200.

As the pressure of wound treatment material "W" within support structure 200 increases, as seen in FIG. 36, circular tube 202 comes into contact with or substantially approaches first intestinal section "T1" and wound treatment material "W" is dispensed from apertures 210. As wound treatment material "W" is dispensed from support structure 200, wound treatment material "W" is deposited on first intestinal section "T1". Preferably, wound treatment material "W" is deposited completely around first intestinal section "T1".

While it is shown and described that support structure 200 is configured to deposit wound treatment material "W" onto first intestinal section "T1", it is envisioned and within the scope of the present disclosure for support structure 200 to be configured to dispense wound treatment material "W" onto second intestinal section "T2".

As seen in FIGS. 36 and 37, following deposition of wound treatment material "W" onto first intestinal section "T1",

19

support structure, and in particular circular tube 202 is deflated by withdrawing wound treatment material “W” through conduit 28b and spokes 204. Support structure 200 may include a suture attached to circular tube 202, which extends through tubular body portion 1022 to the proximal end of apparatus 1000, so that the user in pulling on the suture can collapse and/or remove the structure 200. Alternatively, the support structure 200 may include an elastic, expandable material. With wound treatment material “W” deposited on first intestinal section “T1” and with support structure 200 deflated, anvil member 1026 and tubular body portion 1022 are approximated to approximate first intestinal section “T1” and second intestinal section “T2”. The rotatable grip member 1018 is used to approximate the anvil member 1026 and tubular body portion 1022. When first intestinal section “T1” is in contact with second intestinal section “T2”, wound treatment material “W” is sandwiched therebetween.

Surgical stapling apparatus 1000 is then fired by operating handle member 1012, thereby stapling first intestinal section “T1” to second intestinal section “T2”. Upon firing of surgical stapling apparatus 1000, the staples are expelled from distal end 1022 of body portion 1020 by the staple pusher member (not shown) and driven through first and second intestinal sections “T1 and T2”. Additionally, an annular knife, disposed radially inward of the staple pockets 1024, severs the intestinal tissue radially inwardly of the staple pockets 1024, to thereby complete the anastomosis.

In an alternate method, it is envisioned that the surgical anastomosis procedure may be accomplished without staples. Accordingly, following deposition of wound treatment material “W” onto first intestinal section “T1” and/or second intestinal section “T2”, anvil member 1026 is approximated toward distal end 1022 of body portion 1020 until first intestinal section “T1” contacts second intestinal section “T2” thereby squeezing wound treatment material “W” therebetween. Depending on the particular wound treatment material “W” (e.g., adhesive) used, anvil member 1026 is maintained approximated against distal end 1022 of body portion 1020 for a time sufficient for wound treatment material “W” to cure and begin to adhere first intestinal section “T1” and second intestinal section “T2” with one another. The choice of wound treatment material “W” (e.g., adhesive) will determine the time required to maintain anvil member 1026 approximated against distal end 1022 of body portion 1020.

From the foregoing, it will be appreciated that support structure 200 functions to strengthen the anastomosis and reduce the occurrence of bleeding, leaking and stricture. It is also to be appreciated that the wound treatment material applying structure of the present disclosure may be utilized in a number of other applications and is not limited solely to bowel or bronchus anastomosis.

In one embodiment, it is envisioned that apertures 210 may be areas where tube 202 has been weakened. In this manner, as the pressure within tube 202 increases during inflation, these weakened areas will open up and become apertures 210 and allow for wound treatment material “W” to be dispensed therefrom.

As seen in FIGS. 38 and 39, support structure 200 may be fabricated from a polymeric material and may form a circular or “wagon wheel” shaped structure when in the expanded condition. Desirably, spokes 204 extend radially from central hub 206. In the present embodiment, circular tube 202 of support structure 200 does not include apertures 210 formed therein.

In use, structure 200 is inflated at a location between the two layers of tissue to be anastomosed. In this manner, as will be described in greater detail below, when surgical stapling

20

device 1000 is fired, the staples penetrate and/or puncture circular body 202, thereby releasing wound treatment material “W” between the two layers of tissue, and acts to capture circular tube 202 between the two layers of tissue. The firing of surgical stapling device 1000 then drives the knife to sever spokes 204 from the captured circular tube 202, and thereby leave circular tube 202 in position. The circular tube 202, as well as other portions of structure 200, may be formed from bio-absorbable materials. In an alternate method, when the staples puncture circular body 202, the elasticity of support structure 200 causes circular body 202 and spokes 204 to collapse and/or retract back onto hub 206 of shaft 1028 of anvil assembly 1030, in the manner of a popped balloon.

Circular tube 202 may be constructed from any of the materials listed above for the fabrication of structure 100. Circular tube 202 may be reinforced with a mesh or other material in order to thereby provide additional structural integrity and strength. In addition, when the staples penetrate circular tube 202 the staples may capture the mesh and thereby further help to maintain the patency of the lumen between the two layers of anastomosed tissue.

It is contemplated that structure 200 may be used with a two-part adhesive composition by dividing cavity 202a into two separate chambers with each chamber receiving a respective component of the two-part adhesive composition. Alternatively, it is envisioned that a pair of structures 200 may be mounted to shaft 1028 of anvil assembly 1030, with each structure 200 being fluidly connected to a respective component of the two-part adhesive composition.

In the alternative, the structure 200 in FIGS. 38 and 39 may include a collapsible foam that is attached to shaft 1028 and maintained in a collapsed condition. A wound treatment material is delivered to the foam structure through apertures 1028a, thereby expanding the foam. Desirably, the wound treatment material includes a cross-linking material or is reactive with the foam to form an adhesive or sealant material.

Turning now to FIGS. 40 and 41, a support structure, in accordance with an alternate embodiment of the present disclosure, is generally designated as 300. Support structure 300 is generally an annular balloon 302 secured to stem 1028 of anvil member 1026 at a first end 302a and at a second end 302b. Desirably, first end 302a of annular balloon 302 is secured or attached (e.g., adhered) to stem 1028 at a location distal of port 1028a, and second end 302b of annular balloon 302 is secured or attached (e.g., adhered) to stem 1028 at a location proximal of port 1028a. In this manner, as wound treatment material “W” is transmitted through passage 1028b of stem 1028, wound treatment material “W” exits through ports 1028a and fills cavity 304 of annular balloon 302.

As seen in FIG. 41, annular balloon 302 includes a plurality of apertures or perforations 306 formed along a perimetral edge 310 thereof. Accordingly, as wound treatment material “W” fills cavity 304 and the pressure in cavity 304 builds, wound treatment material “W” begins to dispense from perforations 306. Desirably and in accordance with the present disclosure, annular balloon 302 is configured and dimensioned such that perimetral edge 310 and perforations 306 are disposed between adjacent layers of tissue “T1, T2” (shown in phantom in FIG. 41) which are to be secured to one another.

With reference to FIGS. 42-44, a support structure according to yet another embodiment of the present disclosure is generally designated as 400. Structure 400 may be fabricated from any of the materials listed above for the fabrication of structure 100. Structure 400 may have a planar disk-like first, deflated or unexpanded condition, as seen in FIGS. 42 and 43, and a toroidal second, inflated or expanded condition, as seen in FIG. 44.

21

Structure **400** includes a tubular body portion **402** including a substantially centrally located aperture **404** formed therethrough. Structure **400** is defined by an outer terminal edge **406**, and an inner terminal edge **408** defining the size of aperture **404**. Structure **400** is sized such that when structure **400** is operatively associated with stapling device **1000**, outer terminal edge **406** extends beyond staple retaining pockets **1036** of staple cartridge assembly **1022**. Additionally, aperture **404** of structure **400** is sized to at least receive shaft **1028** of anvil assembly **1030** therethrough.

Body portion **402** of structure **400** defines an internal cavity or chamber (not shown) for receiving a wound treatment material, including, and not limited to, a sealant, adhesive, medicament or the like, therein. A port **420** may be provided on body portion **402** through which fluid may be injected into the cavity thereof.

As seen in FIG. **43**, a fluid delivery device, in the form of a syringe "S", may be used to inject and/or deliver fluid, in the form of a sealant, adhesive, medicament or the like, to the cavity of body portion **402**. As seen in FIG. **44**, when structure **400** is inflated with a fluid, structure **400** may have a toroidal shape. While structure **400** is shown in FIG. **44** as having a toroidal shape, when in the inflated condition, it is envisioned and within the scope of the present disclosure the structure **400** may have a washer-like, cylindrical, spherical or other shape, when in the inflated condition.

Similar to structure **200**, in use, with adhesive structure **400** in the inflated condition and positioned on shaft **1028** of anvil assembly **1030**, tubular body portion **1020** and anvil assembly **1030** are approximated to approximate intestinal sections **66**, **68** and capture annular adhesive structure **400** therebetween. Surgical stapling device **1000** is then fired thereby stapling intestinal sections **66**, **68** to one another. Upon firing of surgical stapling device **1000**, staples are expelled from staple cartridge assembly **1022** and driven through intestinal sections **66**, **68** and body portion **402** thereby puncturing body portion **402** and expelling the fluid therefrom.

From the foregoing, it will be appreciated that the structures of the present disclosure function to strengthen the anastomosis and reduce the occurrence of bleeding, leaking and stricture. It is also to be appreciated that the structures of the present disclosure may be utilized in a number of other applications and is not limited solely to bowel or bronchus anastomosis.

In further embodiments, the structures disclosed above are utilized to adhere the intestinal sections to one another without the use of staples. The adhesive material carried by or incorporated in the body portion of the structure joins the intestinal sections and may also provide a seal against leakage. The device **10** is utilized to approximate the intestinal sections and dispose the structure between the intestinal sections, except that the device **1000** need not house staples therein.

Each structure described above is constructed to deliver a predetermined amount of wound treatment material to the target surgical site. The amount of material to be delivered is site specific. Accordingly, different sized (e.g., different thickness or different volume) structures are contemplated for retaining a different volume or quantity of adhesive therein. In this manner, depending on the particular need and the particular surgical procedure, the surgeon may select a structure containing the needed and/or desired volume or quantity of adhesive therein.

While several particular forms of the structures have been illustrated and described, it will also be apparent that various modifications can be made without departing from the spirit and scope of the present disclosure. For example, it is envi-

22

sioned and within the scope of the present disclosure for an energy-activated wound treatment material, such as, an ultraviolet light activated adhesive, to be used in connection with any of the structures described above. In use, either prior to or following firing of surgical stapling device **10**, energy is applied to the structure. For example, a structure including a UV light-curable adhesive is irradiated with UV light to thereby activate the adhesive.

According to one aspect of the present disclosure, an assembly for disposing a support structure between intestinal sections is provided. The assembly includes an annular surgical stapling device, having an anvil assembly and a tubular body portion. The anvil assembly has an anvil member and a first shaft. The tubular body portion carries a plurality of surgical staples in an annular configuration. The tubular body portion has a second shaft disposed radially inward of the surgical staples. The first shaft of the anvil member is attachable to the second shaft of the tubular body. The assembly further includes a support structure having a generally centrally located aperture for being disposed on one of the first shaft and the second shaft. The support structure includes a material selected from the group consisting of at least one of an adhesive, a sealant, a hemostat, and a medicament.

The support structure is impregnated with the material. The support structure includes an inflatable annular structure and is deployable from a first collapsed position to a second expanded position. Wherein, when in the expanded position, the support structure has a toroidal shape defining an interior space for receiving the material. The annular structure may include a circular tube and a plurality of spokes extending radially inwardly from the circular tube. The interior space of the support structure contains the material.

The material may include a first part of a two-part adhesive and is disposed in a first chamber of the interior space of the support structure. A second part of the two-part adhesive is disposed in a second chamber of the interior space of the support structure. The first part and second part of the material is released from the support structure upon deployment of the staples. The staples may have a second part of the two-part adhesive.

The support structure includes a shape memory material and is deployable from a first collapsed position to a second expanded position. The support structure includes a shape memory alloy.

The support structure may include a first layer and a second layer. The first layer includes a first part of a two-part adhesive and the second layer includes a second part of the two-part adhesive.

The support structure may include a first part of a two-part adhesive and a second part of the two-part adhesive may include a liquid to be applied to the support structure.

According to another aspect of the present disclosure, a method of disposing a structure between tissue sections is provided. The method includes the steps of providing a surgical stapling device having an anvil assembly and a body portion. The anvil assembly has an anvil member and the body portion carrying a plurality of surgical staples and a knife. The method further includes the steps of inserting the anvil assembly into a first tissue section; inserting the body portion in a second tissue section; and disposing a support structure between the first tissue section and the second tissue section, the annular structure including a wound treatment material. The method further including the steps of approximating the anvil assembly and body portion with one another so that an end portion of the first tissue section, an end portion of the second tissue section and the support structure are disposed between the anvil member and the body portion, the

23

support structure being disposed between the first tissue section and the second tissue section; deploying the staples from the body portion; and cutting the first tissue section and the second tissue section with the knife.

The anvil assembly may have a first shaft and the body portion may have a second shaft, wherein the first shaft is attachable to the second shaft. The method further including the step of attaching the first shaft to the second shaft before the step of approximating.

The support structure may have an annular shape and include a generally centrally located aperture. The method further includes the step of inserting one of the first shaft and the second shaft into the aperture before the step of attaching the first shaft to the second shaft. The support structure may be disposed on one of the first shaft and the second shaft before the step of approximating.

The support structure includes a shape memory material and is deployable from a first collapsed position to a second expanded position. The support structure is deployed from the first position to the second position before the step of approximating.

The support structure includes an interior space housing a wound treatment material. The wound treatment material is deployed from the interior space upon deployment of the staples.

The wound treatment material is selected from the group consisting of an adhesive, a sealant and a medicament.

The method further includes the step of deploying an adhesive material. The support structure may include a first layer and a second layer. The step of deploying an adhesive material may include contacting the first layer and the second layer. The support structure may include a first part of a two-part adhesive. Accordingly, the step of deploying an adhesive material may include deploying a second part of the two-part adhesive before the step of approximating. The step of deploying an adhesive material includes puncturing the support structure, wherein the support structure having an interior space containing an adhesive therein.

According to a further aspect of the present disclosure, an assembly for joining tissue is provided. The assembly includes an anvil and a body portion juxtaposed with respect to one another along a shaft and arranged so as to be approximated with respect to one another; and a support structure including a resilient material.

The support structure may include a mesh-like material and the resilient material is woven into the mesh of the support structure. The support structure includes a first layer and a second layer. The resilient material may be disposed between the first layer and the second layer.

The first layer of the support structure includes a first part of a two-part wound treatment material, and the second layer of the support structure includes a second part of the two-part wound treatment material.

The support structure includes a first part of a two-part wound treatment material and a second part of the two-part wound treatment material may include a liquid to be applied to the support structure.

According to one aspect of the present disclosure, an assembly for joining tissue is provided. The assembly includes an anvil and a body portion juxtaposed with respect to one another along a shaft and arranged so as to be approximated with respect to one another; and a support structure on the shaft, the support structure defining a cavity for containing a wound treatment material therein. The support structure may be bio-absorbable.

The body portion may carry a plurality of surgical staples in a circular configuration. The surgical staples are deploy-

24

able against the anvil. The assembly further includes an annular knife disposed radially inwardly of the staples.

The support structure includes an inflatable circular tube. The support structure is deployable from a first collapsed condition to a second expanded condition. The shaft includes at least one port in communication with the cavity for delivering wound treatment material. The wound treatment material expands the support structure from a first collapsed condition to a second expanded condition. The interior space of the circular tube defines a first chamber for receiving a first part of a two-part wound treatment material. The interior space of the circular tube defines a second chamber for receiving a second part of the two-part wound treatment material.

The plurality of surgical staples may have a second part of the two-part wound treatment material.

A support structure for use with an annular stapling apparatus in performing an anastomosis is provided. The support structure includes a disk shaped body portion having an upper surface, a lower surface, an outer terminal edge, and an inner terminal edge defining an aperture therein, the body portion defining a central axis through the aperture; and a first and a second membrane extending radially outward from the outer terminal edge of the body portion.

The inner terminal edge of the body portion extends radially inward of an inner radial edge of a staple cartridge assembly of the stapling apparatus when the support structure is positioned on a shaft of an anvil assembly of the stapling apparatus. The aperture of the body portion is dimensioned to receive a shaft of an anvil assembly.

Each of the first and second membranes is made from a polymeric film. Desirably, each of the first and second membranes is made from polyethylene.

The support structure may have an undeployed condition wherein the first and second membranes are rolled-up towards the body portion, and a deployed condition wherein the first membrane extends in a substantially distal direction from the body portion and the second membrane extends in a substantially proximal direction from the body portion.

The support structure further includes a rip-cord rolled-up into each of the first and second membranes when the support structure is in the undeployed condition. Each rip-cord includes a free end extending from the rolled-up membranes when the support structure is in the undeployed condition. Accordingly, pulling on a rip-cord causes a respective one of the first and second membranes to un-roll. Each of the first and second membranes extends approximately 2.0 cm when un-rolled.

Each membrane includes a first inner layer and a second outer layer. The second outer layer of each membrane swells at a rate greater than the first inner layer.

The support structure may have an undeployed condition wherein the first and the second membranes extend substantially radially outward from the body portion, and a deployed condition wherein the first membrane extends in a substantially distal direction from the body portion and the second membrane extends in a substantially proximal direction from the body portion. Accordingly, when the support structure is in the undeployed condition, the second outer layers of the first and second membranes are in juxtaposed relation to one another.

The second outer layers of the first and second membranes are made from a hydrogel. The first inner layer of each of the first and second membranes is constructed from a substantially non-absorbable material. The first inner layer of each of the first and second membranes is fabricated from a bio-absorbable mesh fabric. Accordingly, when the support structure is positioned on a shaft of an anvil assembly and the anvil

25

assembly is approximated toward a staple cartridge assembly, the support structure is disposed between adjacent tissue sections to be anastomosed. Additionally, when the support structure is disposed between the adjacent tissue sections, as second inner layers of first and second membranes absorb moisture, the first and second membranes curl in the direction of the first inner layer of respective first and second membranes such that the first outer layer contacts a respective tissue section.

According to yet another aspect of the present disclosure, a method of disposing a support structure between adjacent intestinal sections is provided. The method includes the steps of providing an annular surgical anastomosis device. The annular surgical anastomosis device includes an anvil assembly having an anvil member and a first shaft; and a tubular body portion having an annular knife operatively disposed therein and a second shaft disposed radially inward of the annular knife. The first shaft of the anvil assembly is selectively attachable to the second shaft of the tubular body.

The method further includes the steps of inserting the anvil assembly into a first intestinal section; inserting the tubular body portion into a second intestinal section; disposing a support structure between the first intestinal section and the second intestinal section; approximating the anvil assembly and tubular body portion with one another so that an end portion of the first intestinal section, the support structure, and an end portion of the second intestinal section are disposed between the anvil member and the tubular body portion, the support structure being disposed between the first intestinal section and the second intestinal section; and firing the surgical anastomosis device to sever the portions of the first and second intestinal sections disposed radially inward of the annular knife, and to touch the portions of the first and second intestinal sections radially outward of the annular knife against the support structure.

The anvil assembly may include a first shaft and the tubular body portion may include a second shaft disposed radially inward of the annular knife. The first shaft of the anvil member may be attachable to the second shaft of the tubular body portion. The method may further include the step of attaching the first shaft of the anvil assembly to the second shaft of the tubular body portion prior to the step of approximating the anvil assembly to the tubular body portion.

The support structure may include an aperture formed therein. Accordingly, the method may further include the step of inserting one of the first shaft of the anvil assembly and the second shaft of the tubular body portion into the aperture of the support structure prior to the step of attaching the first shaft of the anvil assembly to the second shaft of the tubular body portion.

The tubular body portion may carry a plurality of surgical staples in a circular configuration. The surgical staples are disposed radially outward of the annular knife. Accordingly, upon firing of the anastomosis device, the plurality of staples penetrate a first interstitial section, the support structure and then a second interstitial section.

Desirably, the step of firing the surgical anastomosis device includes driving the plurality of staples from the tubular body portion through the second intestinal section, through the support structure, through the first intestinal section, and against the anvil member.

The support structure includes a disk shaped body portion having an upper surface, a lower surface, an outer terminal edge, and an inner terminal edge defining an aperture therein, the body portion defining a central axis through the aperture; and a first and a second membrane extending radially outward from the outer terminal edge of the body portion. The inner

26

terminal edge of the body portion of the support structure extends radially inward of an inner radial edge of a staple cartridge assembly of the stapling apparatus when the support structure is positioned on the first shaft of the anvil assembly of the surgical anastomosis device. The aperture of the body portion of the support structure is dimensioned to receive the first shaft of the anvil assembly.

Each of the first and second membranes of the support structure may be made from a polymeric film, preferably, polyethylene.

The support structure may have an undeployed condition wherein the first and second membranes thereof are rolled-up towards the body portion, and a deployed condition wherein the first membrane extends in a substantially distal direction from the body portion of the support structure and the second membrane extends in a substantially proximal direction from the body portion of the support structure.

Desirably, a rip-cord may be rolled-up into each of the first and second membranes of the support structure when the support structure is in the undeployed condition. Each rip-cord may include a free end extending from the rolled-up membranes when the support structure is in the undeployed condition.

The method may further include the step of pulling on each rip-cord to unroll the first and second membranes over the first and second intestinal sections. Each of the first and second membranes of the support structure extends approximately 2.0 cm when un-rolled. Each membrane of the support structure includes a first inner layer and a second outer layer. The second outer layer of each membrane of the support structure swells at a rate greater than the first inner layer.

The support structure has an undeployed condition wherein the first and the second membranes extend substantially radially outward from the body portion thereof, and a deployed condition wherein the first membrane extends in a substantially distal direction from the body portion thereof and the second membrane extends in a substantially proximal direction from the body portion thereof. Accordingly, when the support structure is in the undeployed condition, the second outer layers of the first and second membranes are in juxtaposed relation to one another.

The second outer layers of the first and second membranes are made from a hydrogel. The first inner layer of each of the first and second membranes of the support structure is constructed from a substantially non-absorbable material. The first inner layer of each of the first and second membranes is fabricated from a bio-absorbable mesh fabric.

The support structure is positioned on the first shaft of the anvil assembly and the anvil assembly is approximated toward the staple cartridge assembly, the support structure is disposed between adjacent tissue sections to be anastomosed.

Desirably, when the support structure is disposed between the adjacent tissue sections, as second inner layers of first and second membranes absorb moisture, the first and second membranes curl in the direction of the first inner layer of respective first and second membranes such that the first outer layer contacts a respective intestinal section.

The first and second membranes of the support structure desirably extend approximately 2.0 cm from the outer terminal edge of the body portion of the support structure.

According to yet another aspect of the present disclosure, an anvil assembly for use with and operatively connectable to an annular surgical stapling device is provided. The anvil assembly includes an anvil member; a shaft extending from the anvil member; and a support structure assembly operatively supported on the shaft. The support structure assembly includes a sleeve defining a chamber therein, the sleeve being

27

movable along the length of the shaft; and a support structure. The support structure includes a hub operatively supported on the shaft; a plurality of spokes extending from the hub; a disc supported on the spokes; and wound treatment material associated with the disc.

The sleeve is axially movable along the length of the shaft from a first position in which the support structure is in a collapsed condition and contained in the chamber of the sleeve and a second position in which the support structure is in an expanded condition and free from the sleeve.

The spokes are fabricated from a shape memory material. The disc is fabricated from a mesh. The disc is bio-absorbable. The reinforcing member may further include a ring connected to the spokes. The ring is fabricated from a shape memory material.

The wound treatment material is at least one of an adhesive, a sealant, a hemostat and a medicament. The adhesive is at least one of a protein derived, aldehyde-based adhesive material, and a cyanoacrylate-based material. The sealant is at least one of a fibrin sealant, a collagen-based and synthetic polymer-based tissue sealant, a synthetic polyethylene glycol-based sealant, and a hydrogel material. The hemostat material is at least one of a fibrin-based, a collagen-based, an oxidized regenerated cellulose-based and a gelatin-based topical hemostat, and fibrinogen-thrombin combination materials. The medicament is at least one of a drug, an enzyme, a growth factor, a peptide, a protein, a dye, a diagnostic agent and a hemostasis agent.

The sleeve may include a cam surface formed therein and the shaft includes a cam follower provided thereon, wherein the cam follower is configured to ride in the cam surface.

It is further contemplated that each of the structures described herein may be used with an annular surgical anastomosing device, not including any staples for securing tissue together, which is capable of approximating, adhering and cutting tissue.

Thus, it should be understood that various changes in form, detail and application of the structures of the present disclosure may be made without departing from the spirit and scope of the present disclosure.

28

What is claimed is:

1. An assembly for joining tissue, comprising:

an anvil and a body portion juxtaposed with respect to one another along a shaft and arranged so as to be approximated with respect to one another;

the body portion carrying a plurality of surgical staples in an annular configuration, the surgical staples being deployable against the anvil;

a support structure connected to the shaft, the support structure defining a cavity for containing a wound treatment material therein;

the shaft including at least one port in communication with the cavity for delivering the wound treatment material; and,

an annular knife disposed radially inwardly of the surgical staples.

2. The assembly according to claim 1, wherein the support structure is bio-absorbable.

3. The assembly according to claim 1, wherein the support structure includes an inflatable annular tube.

4. The assembly according to claim 1, wherein the support structure is deployable from a first collapsed condition to a second expanded condition.

5. The assembly according to claim 1, wherein wound treatment material expands the support structure from a first collapsed condition to a second expanded condition.

6. The assembly according to claim 3, wherein an interior space of the annular tube defines a first chamber for receiving a first part of a two-part wound treatment material.

7. The assembly according to claim 6, wherein the interior space of the annular tube defines a second chamber for receiving a second part of the two-part wound treatment material.

8. The assembly according to claim 6, wherein the plurality of surgical staples have a second part of the two-part wound treatment material.

* * * * *