



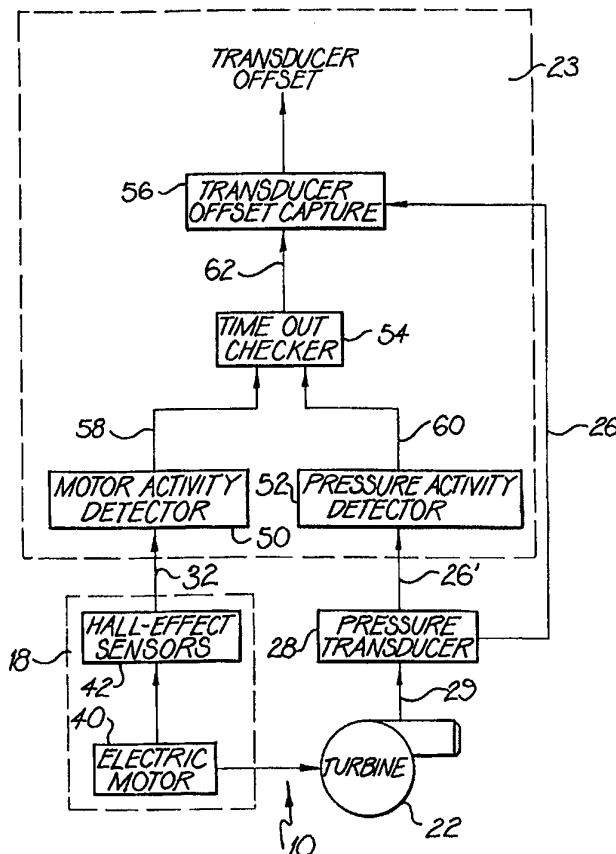
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<p>(21) International Application Number: PCT/AU96/00413 (22) International Filing Date: 3 July 1996 (03.07.96) (30) Priority Data: PN 3948 3 July 1995 (03.07.95) AU (71) Applicant (for all designated States except US): RESMED LIMITED [AU/AU]; 82 Waterloo Road, North Ryde, NSW 2113 (AU). (72) Inventors; and (75) Inventors/Applicants (for US only): SURJADI, Hary, Soesanto [AU/AU]; 14 Truscott Avenue, Kariang, NSW 2250 (AU). FINN, Shane, Darren [AU/AU]; 4 Sophia Crescent, North Rocks, NSW 2151 (AU). COLLA, Gregory, Alan [AU/AU]; 2A Doris Street, North Sydney, NSW 2060 (AU). (74) Agent: SPRUSON & FERGUSON; G.P.O. Box 3898, Sydney, NSW 2001 (AU).</p>		<p>(81) Designated States: AL, AM, AT, AU, AZ, BB, BG, BR, BY, CA, CH, CN, CZ, DE, DK, EE, ES, FI, GB, GE, HU, IL, IS, JP, KE, KG, KP, KR, KZ, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, TJ, TM, TR, TT, UA, UG, US, UZ, VN, ARIPO patent (KE, LS, MW, SD, SZ, UG), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG). Published With international search report.</p>

(54) Title: AUTO-CALIBRATION OF PRESSURE TRANSDUCER OFFSET

(57) Abstract

A flow generator (10) and having use in the provision of CPAP or assisted ventilation treatment is disclosed. The flow generator (10) has a turbine (22) for the supply of breathable gas which is driven by an electric motor (18) and an associated motor power supply (20). The power supply (20) in tune is controlled by a controller (23). A pressure sensing port (27) measures delivery pressure that is passed to a pressure transducer (28), the output signal of which is passed to the motor controller (23). The zero offset of the pressure transducer (28) is automatically calibrated on occurrence of the conditions where the turbine (22) is not operating and no pressure activity is sensed by the transducer (28). The turbine not operating condition can be determined from Hall-effect sensors (42) integral of the motor (18).



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AUTO-CALIBRATION OF PRESSURE TRANSDUCER OFFSET

Field of the Invention

This invention relates to the auto-calibration of pressure transducers. In one preferred form, it relates to pressure transducers for use in apparatus for the provision of Continuous Positive Airway Pressure (CPAP) treatment to patients suffering from Obstructive Sleep Apnea (OSA) and for use in apparatus for ventilating assistance.

Background of the Invention

CPAP is a well known treatment for the temporary relief of conditions including obstructive sleep apnea (OSA) and snoring. By this technique, air (or breathable gas) at a pressure elevated above atmospheric pressure is continuously supplied to the entrance of a patient's airway (by the nasal and/or oral route) by means of known arrangements of masks or nasal prongs. The elevated air pressure acts as a pneumatic splint of the patient's airway in the vicinity of the oro- and hypo-pharynx, reducing or eliminating the occurrences of apneas or hypopneas during sleep. A bi-level CPAP device, as opposed to a constant treatment level CPAP device, delivers two distinct pressures during the patient's respiratory cycle - a relatively lower pressure during exhalation and a relatively higher pressure during inhalation. In another form, an automatically adjusting CPAP device may operate to provide a relatively low background pressure which increases to a therapeutic pressure on a needs basis, and preferably at a time to prevent the onset of an apnea.

The term "CPAP" used herein thus is to be understood as including constant, bi-level or adjusting forms of continuous positive airway pressure.

Common to all forms of CPAP apparatus is a nose, mouth or face mask which is fitted to a patient and connected to a flow generator via a flexible air delivery tube/conduit. The flow generator includes an electric motor driving a turbine to provide a supply of air or breathable gas for the administration of CPAP treatment

during sleep. The range of positive air pressures supplied at the entrance to a patient's airway typically is in the range 2 - 20 cm H₂O. In the pressure regulation control of the flow generator it is usual to have a continuous measure of mask or flow generator delivery pressure, commonly achieved by locating a pressure sensing port at the mask
5 or proximate the flow generator outlet.

In the clinical assessment of the severity of a patient's OSA or upper airway syndrome condition, it is desired to identify the minimum possible CPAP treatment pressure that will alleviate the occurrence of partial or complete apneas during sleep. This is for the reason that the patient is required to expend respiratory effort in
10 expiration against the positive airway pressure, hence it is preferable to minimise the work that must be done to ensure quality of sleep, and as follows administer only the minimal necessary CPAP treatment pressure. In this regard, it is important that the pressure transducer being used to measure the CPAP treatment pressure in control of the flow generator has satisfactory electro-mechanical characteristics so that the set-
15 point CPAP treatment pressure does not vary significantly. It is known that a reduction of CPAP treatment pressure of as little as 1 cm H₂O can nullify the therapeutic effect and result in a patient experiencing apneas during sleep.

There is, not unexpectedly, a direct correlation between the electro-mechanical performance of pressure transducers and price, hence the need for accurate
20 pressure measurement is antagonistic towards the need to be able to manufacture CPAP apparatus at a cost that is acceptable to the marketplace. Commercially available pressure transducers, that are not extraordinarily expensive, operate in a small part of their pressure dynamic range in CPAP applications, meaning that there can be a 5-10% drift in the measured value with time due wholly to a pressure transducer operating in a
25 'stretched' region of operation. Such a variation translates to a variation in CPAP treatment pressure of about 1 - 2 cm H₂O. There further is market pressure for CPAP treatment to be determined to within an accuracy as low as 0.1 cm H₂O.

It is therefore one preferred object of the invention to be able to avoid the need to incorporate expensive pressure transducers in CPAP apparatus and yet still maintain accurate monitoring of, and control over, CPAP treatment pressure.

A similar consideration applies for ventilators or apparatus for assisted
5 ventilation that provide breathable gas to a patient at a controlled pressure. The gas is delivered to the patient, in the case of a ventilator, by way of a mask or an endotracheal tube. Patients with lung disease, neuromuscular disease, chest wall disease, or abnormalities of respiratory control may require ventilatory assistance. This is because they have various combinations of elevated airway resistance, stiff lungs and chest wall,
10 ineffective respiratory muscles, or insufficient neural activation of the respiratory muscles. The need for ventilatory assistance is particularly common during sleep. Pressure controlled, time triggered ventilators, for example, deliver a relatively high inspiratory pressure (IPAP) for a fixed period of time (TI), and a relatively low expiratory pressure (EPAP) for another fixed period of time (TE). The cycle is then
15 repeated indefinitely.

Pressure transducers typically are factory calibrated before delivery, to establish a zero pressure value (with respect to CPAP treatment pressure that is relative to atmospheric pressure) in terms of the transducer's offset or bias. The "zero offset value" thus corresponds to atmospheric pressure. Even so, due to the inherent
20 variations in the transduced pressure, and due to aging of the transducer and its temperature dependency, the preset offset value can vary by the equivalent of ± 1 cm H₂O leading to measurement error. This means that the patient must periodically return the CPAP apparatus to the manufacturer or servicer for re-calibration, else perform a re-calibration procedure themselves, possibly requiring venting of the
25 transducer to atmospheric pressure. It is therefore another preferred object of the invention to provide for auto-calibration of pressure transducer offset.

For convenience any reference to a "mask" hereafter is to be understood as including nasal, oral or face masks, and nasal prongs.

Summary of the Invention

The present invention is directed to methods and apparatus whereby one or more of the foregoing problems can be overcome or at least ameliorated.

5 Therefore, in a broad form the invention discloses a method for auto-calibration of the offset of a pressure transducer for use in CPAP or pressure regulated ventilation apparatus, the CPAP apparatus comprising a flow generator operable to supply breathable gas to a delivery tube in turn connected to a patient mask, and the pressure transducer measuring delivery pressure in the mask, delivery tube or flow
10 generator, the method comprising the steps of:

determining whether the flow generator is operating;

determining whether there is no pressure activity sensed by the transducer; and

if both determinations are satisfied, accepting the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.

15 The invention further discloses a method for auto-calibration of the offset of a pressure transducer for use in CPAP or pressure regulated ventilation apparatus, the apparatus comprising a flow generator operable to supply breathable gas to a delivery tube in turn connected to a patient mask, and the pressure transducer measuring delivery pressure in the mask, delivery tube or flow generator, the method comprising
20 the steps of:

determining whether no pressure activity is continuously sensed by the transducer over a predetermined period of time, and if so accepting the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.

The invention yet further discloses a flow generator for the supply of
25 breathable gas comprising an electric motor driving a turbine, control circuitry, a pressure transducer to sense delivery pressure at or remote from said flow generator and whose electrical output is connected to said control circuitry, and sensing means connected to said control circuitry, and wherein said control circuitry is operable to

determine from said sensing means whether the electric motor or the turbine are operating and from the pressure transducer whether there is no pressure activity, and if both determinations are satisfied, to accept the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.

5 The invention yet further discloses a flow generator for the supply of breathable gas comprising an electric motor driving a turbine, control circuitry, and a pressure transducer to sense delivery pressure at or remote from said flow generator and whose electrical output is connected to said control circuitry, and wherein said control circuitry is operable to determine from the pressure transducer whether there is
10 no pressure activity continuously over a predetermined period of time, and if so, to accept the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.

 An auto-calibration thus can be performed in the sense that there is no user/patient involvement nor manual activation, rather performance by the flow
15 generator autonomously. If either determination is not met an auto-calibration is not performed.

 The pressure offset value is applied to all subsequent pressure measurements to determine treatment pressure. Preferably, the two determinations are made over a plurality of successive instances and must both be satisfied on each instance before
20 accepting the updated offset value.

 In a preferred form, the current pressure value is compared against a preceding pressure value, and if differing less than a predetermined threshold then there is pressure inactivity. The preceding pressure value can be a running or moving average of such values.

25 The electric motor operation sensing means can be Hall-effect sensors integral of, or mounted to the electric motor. The flow generator can further comprise power supply means being controlled by the control circuitry and having control of the rotational speed of the electric motor.

The invention further discloses a flow generator as described, and a delivery tube coupled thereto and to a patient mask. The mask can be a nose, mouth or face mask. The pressure sensing port can be located at the turbine exit, a point along the tube or at the mask.

5 In one preferred form, the invention can be said to involve methods and apparatus for providing auto-calibration of pressure transducer offset that is implemented by continuously monitoring the flow generator electric motor to determine whether it is running and monitoring the pressure transducer for respiratory activity. If the motor is not running, and no pressure activity is detected, then the pressure
10 measured by the transducer is determined to be atmospheric pressure, and so the electrical output from the transducer represents the zero pressure offset. The offset value at this point in time is stored to be subtracted from any subsequent pressure measurement values to determine treatment pressure.

In an alternate embodiment, auto-calibration of pressure transducer offset is
15 implemented by determining whether there is no pressure activity sensed by the pressure transducer over a continuous period that is long compared with physiological events such as respiration and apnea. This single determination thus subsumes the separate determinations of motor operation and respiratory activity.

The zero offset can be updated whenever the opportunity arises, thus taking
20 into account effects due to transducer ageing and temperature effects. In this way, the magnitude of a transducer's offset error can be determined automatically without the need for additional hardware elements, such as a solenoid-operated valve venting the transducer to atmospheric. There also is no need for any user intervention in the periodic re-calibration. This leads to a reduction in the cost of the hardware
25 components of a CPAP or pressure regulated ventilation apparatus, and to a reduced manufacturing unit cost due to a reduction in labour required, for reason of there being no need to manually calibrate a transducer at the factory in advance of shipment, in combination resulting in reduced cost of the apparatus to the patient.

The improved pressure measurement accuracy gained also has therapeutic benefit, in that the CPAP or ventilation treatment will remain effective for a patient, in that the clinically-determined delivery pressure is maintained with accuracy.

5 **Description of the Drawings**

An embodiment of the invention now will be described with reference to the accompanying drawings, in which:

Fig. 1 is a schematic block diagram of CPAP apparatus as used for the treatment of OSA;

10 Fig. 2 is a schematic block diagram representative of hardware components constituting an embodiment of the invention;

Fig. 3 is a schematic block diagram of representative computational steps in performance of the embodiment;

15 Fig. 4 is a schematic block diagram representative of hardware components constituting another embodiment;

Fig. 5 is a schematic block diagram of representative computational steps in performance of another embodiment; and

Fig. 6 shows a typical pressure waveform during calibration.

20 **Detailed Description of Preferred Embodiments and Best Mode**

The embodiment to be described relates to CPAP apparatus, however it is to be understood that other embodiments are equally applicable in the field of pressure regulated ventilators.

25 Referring then to Fig. 1, the CPAP apparatus comprises a flow generator 10 coupled by a flexible delivery tube or conduit 12, in this case, to a nose mask 14 worn by a patient 16. The flow generator 10 broadly comprises an electric motor 18 that is powered by a motor power supply 20. In turn, the electric motor 18 has mechanical coupling with a turbine 22 that outputs either air or breathable gas at a pressure

elevated above atmospheric pressure to the delivery tube 12. The output delivery pressure from the turbine 22 is governed by the rotational speed of the electric motor 18. The speed thus is the "controlled variable" relative to the desired CPAP treatment pressure. The motor 18 speed is controlled by the motor controller 23 which effects
5 changes in motor speed by means of a control signal on control line 24 provided to the motor power supply 20. Accordingly, motor speed is controlled by means of varying the motor power supply 20, typically in output voltage and/or duty cycle.

The motor controller 23 receives an electrical signal on control line 26 in this case representative of delivery pressure from the turbine 22 as measured by the
10 pressure transducer 28, which is connected via a sensing line 29 to a sensing port 27 proximate to the turbine outlet. In an alternative form, the pressure transducer 28 can be connected via a sensing line 29' to a sensing port 27' located at the nose mask 14.

In the event of the transducer 28 being located at the turbine 22 outlet, it is necessary for the motor controller to be able to compensate for pressure losses (as a
15 function of flow) along the delivery tube 12, since ultimately it is the pressure at the entrance to the airway that is to be monitored and controlled to ensure effective CPAP treatment. This compensation can be performed by empirical measurement or by a knowledge of the flow vs pressure characteristic of the delivery tube 12.

In one preferred form, the turbine 22 can be a PAPST™ ECA 27-11 brushless
20 DC motor. Being a DC motor, its speed is directly proportional to the armature voltage. The particular motor described has integral Hall-effect sensors, thus providing a measure of motor angular rotational speed, that signal being output from the motor 18 to the motor controller 22 on control line 30.

The pressure transducer 28 can be such as a Motorola™ MPX 2010DP type.
25 The motor controller 23 can be implemented by any commercially available microprocessor, although one preferred form is the 8-bit Motorola™ MC68HC805B6 micro-controller.

When the motor 18 is not running, hence the turbine 22 is not rotating to produce pressurised air or breathable gas, if the nose mask 14 is not being worn then the air pressure measured by the transducer 28 will be atmospheric pressure. The transducer 28 will have an electrical output in response only to atmospheric pressure.

5 The measurement obtained of atmospheric pressure represents the "zero offset" value, and hence the motor controller 23 must be calibrated to take into account this zero offset so accurate measurements can be performed. That "zero offset" output must be subtracted from a pressure value measured with the turbine 22 rotating in order to obtain a measurement of CPAP delivery pressure.

10 As previously discussed, the electrical performance of pressure transducers varies over time, and whilst the linearity may remain essentially constant, the zero offset can vary by 5 - 10%. The present embodiment operates to auto-calibrate the transducer in terms of the "zero offset" at available times, viz., occasions when the flow generator 10 is not being operated and the mask 14 is not being worn (or there is

15 no respiration) by the patient 16.

In Fig. 2 the elements common with Fig. 1 are shown using like reference numerals. The electric motor 18 is represented by the component motor 40 and integral Hall-effect (speed) sensors 42. Within the dashed box representing the motor controller 23, only some number of the logic elements constituting the controller have been

20 shown. These logic elements are the ones involved in generation of a "Transducer Offset" signal that equates to the "zero offset" value of the transducer and thus atmospheric pressure.

The output signal from the speed sensors 42 is passed on a control line 32 to a motor activity detector 50, and the signal representing the measured pressure appears

25 on another control line 26 to be passed to a pressure activity detector 52. Both the motor activity detector 50 and the pressure activity detector 52 pass logic signals on respective lines 58,60 to a time-out checker 54, the output from which is passed on a line 62 to a transducer offset capture element 56 that also receives the output of the

pressure transducer 28. These two signals are processed to generate the "Transducer Offset" value to be passed to other processing elements of the motor controller 23.

Reference now will be made to the flow diagram of Fig. 3 and the logic and computational steps therein that further describe the present embodiment. These steps are performed by the motor controller 23 in the form of either a stored computer program in machine readable form or discrete logic elements. Step 60 determines whether a warm-up period has elapsed to allow the flow generator 10 to reach a normal operating temperature. A typical minimum warm-up time is 15 minutes. If this step is satisfied, the "pressure activity counter" is reset (i.e. to zero) in step 62, followed by step 64 that determines whether the motor 40 is operating/running. This step is performed through use of the Hall-effect sensors 42 and the motor activity detector 50. If the motor is running, it is not possible to perform the auto-calibration. If the motor is not running, step 66 determines whether any pressure activity is sensed. This is achieved by way of the pressure transducer 28 and the pressure activity detector 52. If there is pressure activity then again the auto-calibration cannot be performed. Pressure activity can be defined as an absolute difference between two consecutively measured pressure samples exceeding a predetermined threshold. In this regard the immediately preceding value is stored and compared with the current value. The difference is compared with a predetermined threshold, typically set to $\pm 0.5\%$ (approximately equivalent to 1 count in a range of 185 counts). If the threshold is not exceeded, it is determined there is no pressure activity.

If no pressure activity is sensed, then in step 68 the "pressure inactivity counter" is incremented. In step 68 the value of the pressure inactivity counter is compared against a "pressure inactive time-out" value (viz., by the time-out checker 54) that is implemented to ensure that there is a minimum duration of no motor activity and no pressure activity before auto-calibration can take place. Thus the tests of steps 64 and 66 must be satisfied more than once in the looped-manner shown before the test of

step 70 will be satisfied and, as indicated in step 72, the current pressure transducer output is captured and utilised as an auto-calibration of the Transducer Offset.

The pressure inactive time-out value preferably may be a number of interactions equivalent to, say, a two second duration.

5 The absence of pressure activity corresponds to the absence of respiration, which, in most every case, will be due to the mask 14 not being worn. The only practical instance of there being a lack of pressure activity with the mask being worn is if the patient has ceased breathing, whether that is a consequence of occurrence of an apnea or otherwise. In any event, it would be even rarer for a patient to be wearing a
10 mask during sleep without the electric motor 40 operating.

The "motor not running" condition and the "mask not being worn" condition will tend to occur when the flow generator 10 is first turned on, or may arise from the patient stopping the flow generator, or the flow generator automatically stopping itself in the presence of sensing 'mask off' (whether that be intentional or otherwise).

15 By the methodology described, the Transducer Offset can be updated every two seconds (for example) when the motor 40 is not operating and the mask is not being worn, in that these conditions are satisfied many times over before the time-out period elapses, but only the pressure value immediately preceding the end of the time out period is captured as the updated Transducer Offset.

20 In other embodiments it may be preferred to utilise a running or moving average of previous (say, at least five) pressure samples compared with the current pressure sample to determine whether there is pressure inactivity. Such averaging functions can be achieved by the introduction of appropriate software or hardware filters.

25 In a further embodiment, it may be chosen to base the auto-calibrating Transducer Offset value not upon the instantaneous (atmospheric) sensed pressure, but upon some averaged representation of sensed pressure over a contemporaneous historical period.

In a yet further embodiment, it may also be chosen to separately store the transducer offset measured prior to satisfying the warm-up condition in step 60 so that both a "cold-offset" and a "warm-offset" are stored.

An alternative embodiment is shown with reference to Figs. 4 and 5. In this
5 embodiment the determination of whether the flow generator 10 is in a condition such that auto-calibration can take place occurs on the basis only of the pressure measured by the pressure transducer 28. That is, a determination of the CPAP mask not being worn and the turbine 22 not operating can be arrived at based only on the pressure measurement.

10 The steps shown in Fig. 5 are common with the steps previously shown in Fig. 3, but for omission of the "motor running" step 64. The other difference occurs in relation to step 70, inasmuch as the "time out" value is set to be long with respect to any physiological event. Typical physiological events are respiration and apneas. A time out period of between 2-5 minutes has been determined to be satisfactory.

15 In the event that a patient mask is not being worn and the electric motor 40 is operating to cause rotation of the turbine 22, then for reasons of the flow of air past the pressure transducer 28 to be discharged from the mask into free space, it is the case that fluctuations or perturbations in pressure will be sensed by the pressure transducer 28 to even to fluid dynamics effects in the physical vicinity of the pressure transducer
20 28. A minimum threshold of 0.1 cm H₂O can be utilised to discriminate between pressure activity and pressure inactivity.

Fig. 6 shows a waveform of pressure versus time for the embodiment of Figs. 2 and 3, where the time axis is in 10 seconds per division increments. The waveform represents the signal measured by the pressure transducer 28 with the internal pressure
25 offset applied to provide relative treatment pressure. Time interval A represents the situation of the flow generator 10 being turned off, in which case the measured pressure is 0 cm H₂O relative to atmospheric pressure. Time interval B represents the flow generator stepping up to the minimum CPAP pressure of 4 cm H₂O then ramping to the

target treatment pressure of 7 cm H₂O. Time interval C represents continuous operation at the desired treatment pressure. At the end of time interval C, an artificial offset error is introduced so that the actual pressure generated is 10 cm H₂O whereas the flow generator believes the delivery pressure is 7 cm H₂O. Thus a 3 cm H₂O error
5 in the transducer offset has been introduced. Time interval D represents the continuing operational period with the error in transducer offset. At the end of interval D the flow generator is turned off, and in interval E, the pressure reduces to 0 cm H₂O.

In time interval F two calibration operations are performed. Immediately at the commencement of the interval (upon turning on of the flow generator), the pressure
10 transducer offset value is recalibrated given that the two conditions of the flow generator not operating and there being no pressure activity are satisfied. What follows is a period in which the flow generator operates at approximately 15 cm H₂O, this being a gain calibration that is not directly applicable to the present invention. After the gain calibration, the flow generator again turns off, with the pressure returning to
15 the 0 cm H₂O level. Time interval G represents a ramping-up to resumption of CPAP treatment in interval H at the now correct delivery pressure level of 7 cm H₂O.

CLAIMS:

1. A method for auto-calibration of the offset of a pressure transducer for use in CPAP or pressure regulated ventilation apparatus, the apparatus comprising a
5 flow generator operable to supply breathable gas to a delivery tube in turn connected to a patient mask, and the pressure transducer measuring delivery pressure in the mask, delivery tube or flow generator, the method comprising the steps of:
determining whether the flow generator is operating;
determining whether there is no pressure activity sensed by the transducer; and
10 if both determinations are satisfied, accepting the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.
2. A method as claimed in claim 1, whereby said no pressure activity is determined by the further step of determining whether there is no absolute difference
15 between two consecutive measurements of pressure by the pressure transducer.
3. A method as claimed in claim 2, whereby said no absolute difference between two consecutive measurements of pressure is determined by the further steps of comparing a stored immediately preceding measured pressure value with a current
20 pressure value, comparing the difference against a threshold, and if the threshold is not exceeded, there is no pressure activity.
4. A method as claimed in any one of claims 1 to 3, whereby said flow generator not operating is determined by detecting near zero rotational speed of the
25 flow generator.

5. A method as claimed in any one of claims 1 to 3, whereby said flow generator not operating is determined by there being no sensed pressure activity over a continuous period of time that is long compared with any physiological event.

5 6. A method for auto-calibration of the offset of a pressure transducer for use in CPAP or pressure regulated ventilation apparatus, the apparatus comprising a flow generator operable to supply breathable gas to a delivery tube in turn connected to a patient mask, and the pressure transducer measuring delivery pressure in the mask, delivery tube or flow generator, the method comprising the steps of:

10 determining whether no pressure activity is continuously sensed by the transducer over a predetermined period of time, and if so accepting the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.

7. A method as claimed in claim 6, whereby the period of time is long
15 compared with any physiological event.

8. A flow generator for the supply of breathable gas comprising an electric motor driving a turbine, control circuitry, a pressure transducer to sense delivery pressure at or remote from said flow generator and whose electrical output is
20 connected to said control circuitry, and sensing means connected to said control circuitry, and wherein said control circuitry is operable to determine from said sensing means whether the electric motor or the turbine are operating and from the pressure transducer whether there is no pressure activity, and if both determinations are satisfied, to accept the output of the transducer as a calibrated pressure offset value
25 representative of atmospheric pressure.

9. A flow generator as claimed in claim 8, wherein the control circuitry is further operable to determine whether there is no absolute difference between two consecutive measurements of pressure by the pressure transducer.

5 10. A flow generator as claimed in claim 9, wherein the control circuitry includes a storage element to store an immediately preceding measured pressure value, a difference element to compare the immediately preceding measured value with a current pressure value, and a decision element for determining whether the difference does not exceed a threshold for there to be no pressure activity.

10

11. A flow generator as claimed in any one of claims 8 to 10, wherein the control circuitry includes a difference element to compare a signal from the sensing means against a zero value, and operable to determine the motor or the turbine not to be operating if, as a result of the comparison, the sensing means signal is near zero.

15

12. A flow generator as claimed in claim 11, wherein the sensing means senses rotational speed of the motor or the turbine.

13. A flow generator as claimed in claim 12, wherein the sensing means is
20 one or more Hall-effect sensors.

14. A flow generator for the supply of breathable gas comprising an electric motor driving a turbine, control circuitry, and a pressure transducer to sense delivery pressure at or remote from said flow generator and whose electrical output is
25 connected to said control circuitry, and wherein said control circuitry is operable to determine from the pressure transducer whether there is no pressure activity continuously over a predetermined period of time, and if so, to accept the output of the transducer as a calibrated pressure offset value representative of atmospheric pressure.

15. A flow generator as claimed in claim 14, wherein said predetermined period of time is long compared with any physiological event.

5 16. CPAP or pressure regulated ventilation apparatus comprising a flow generator as claimed in any one of claims 8 to 15, a delivery tube coupled at one end to the turbine and a patient mask coupled at the other end to the delivery tube, the transducer sensing delivery pressure at the turbine, in the delivery tube or at the mask, and the control circuitry operable to determine treatment pressure from the delivery
10 pressure minus said calibrated pressure offset value.

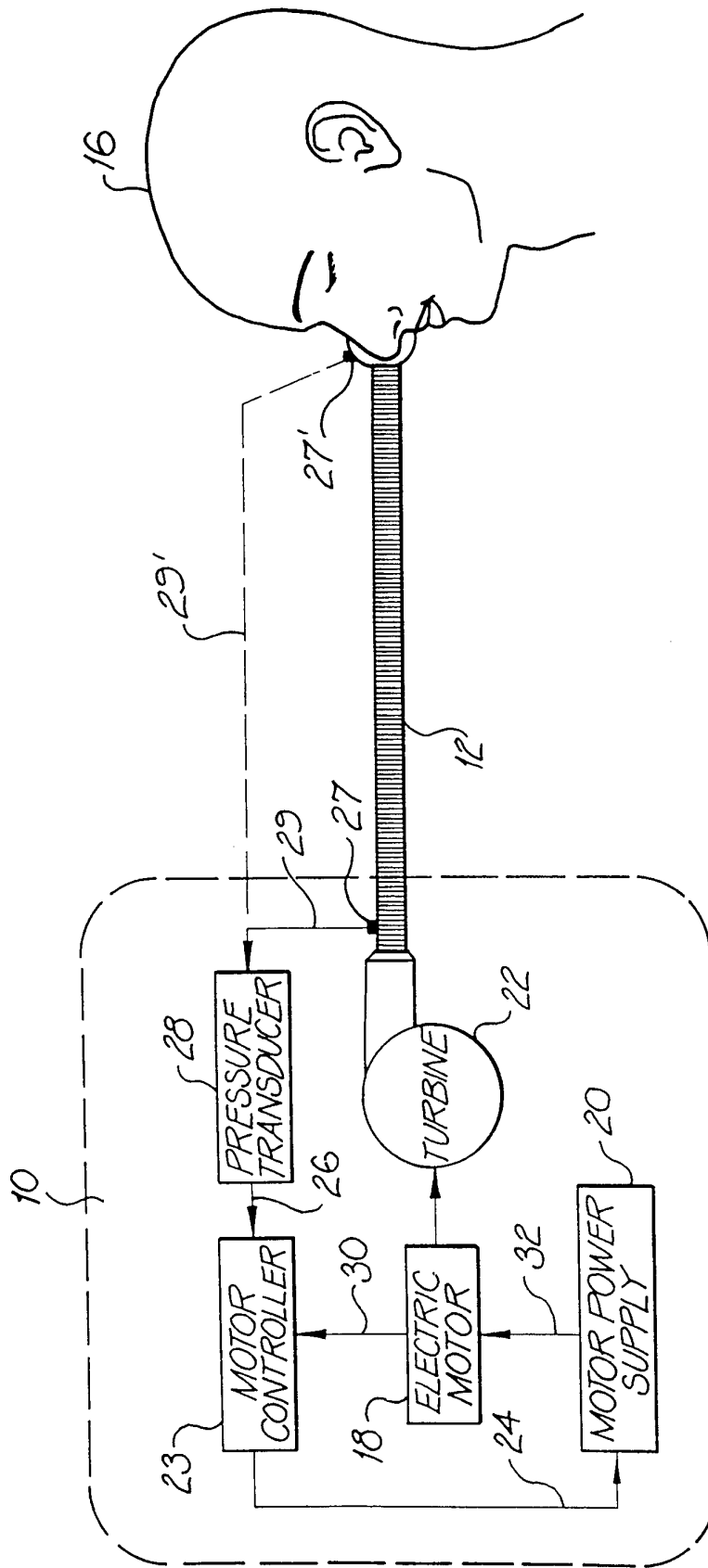


FIG. 1

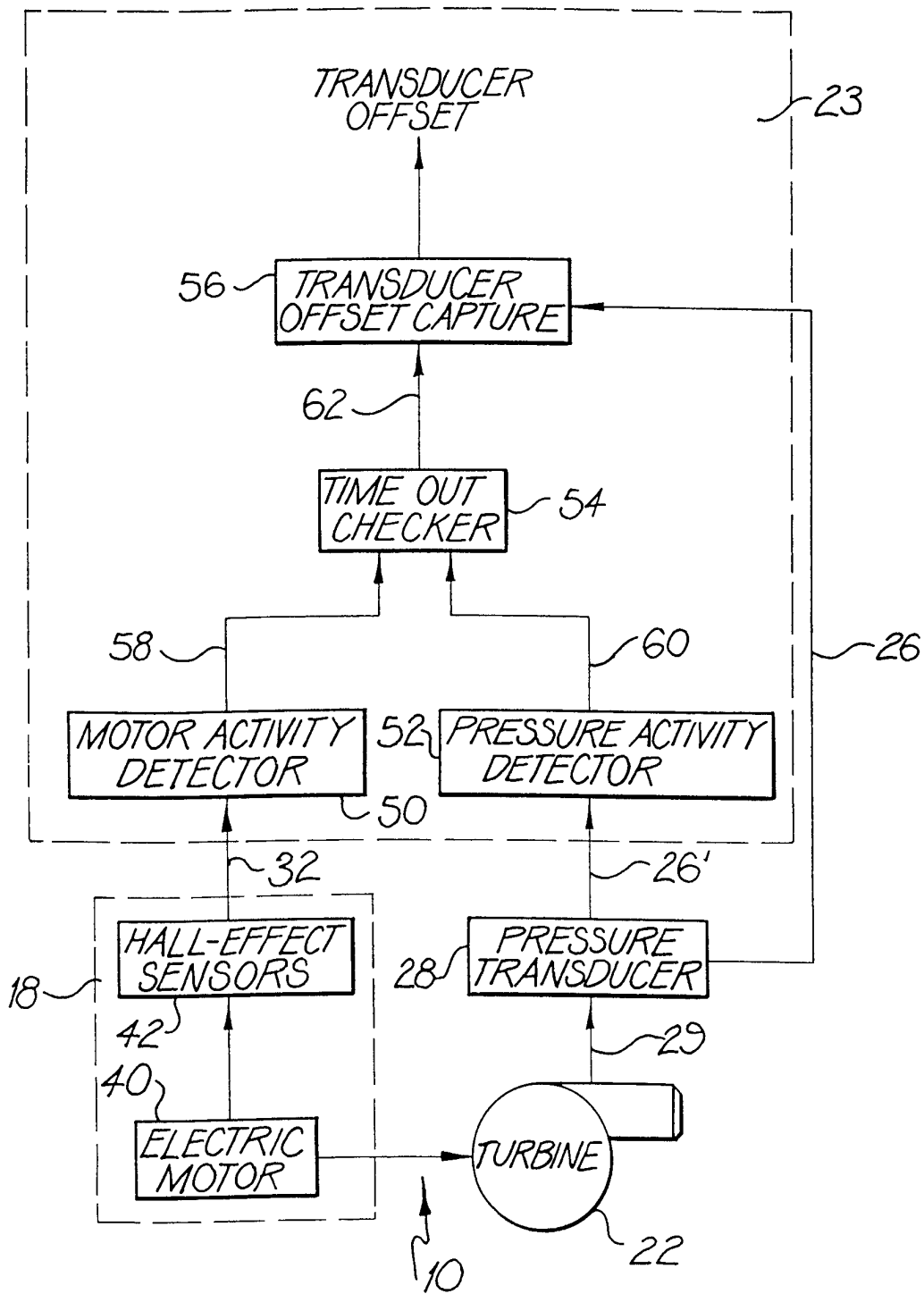


FIG. 2

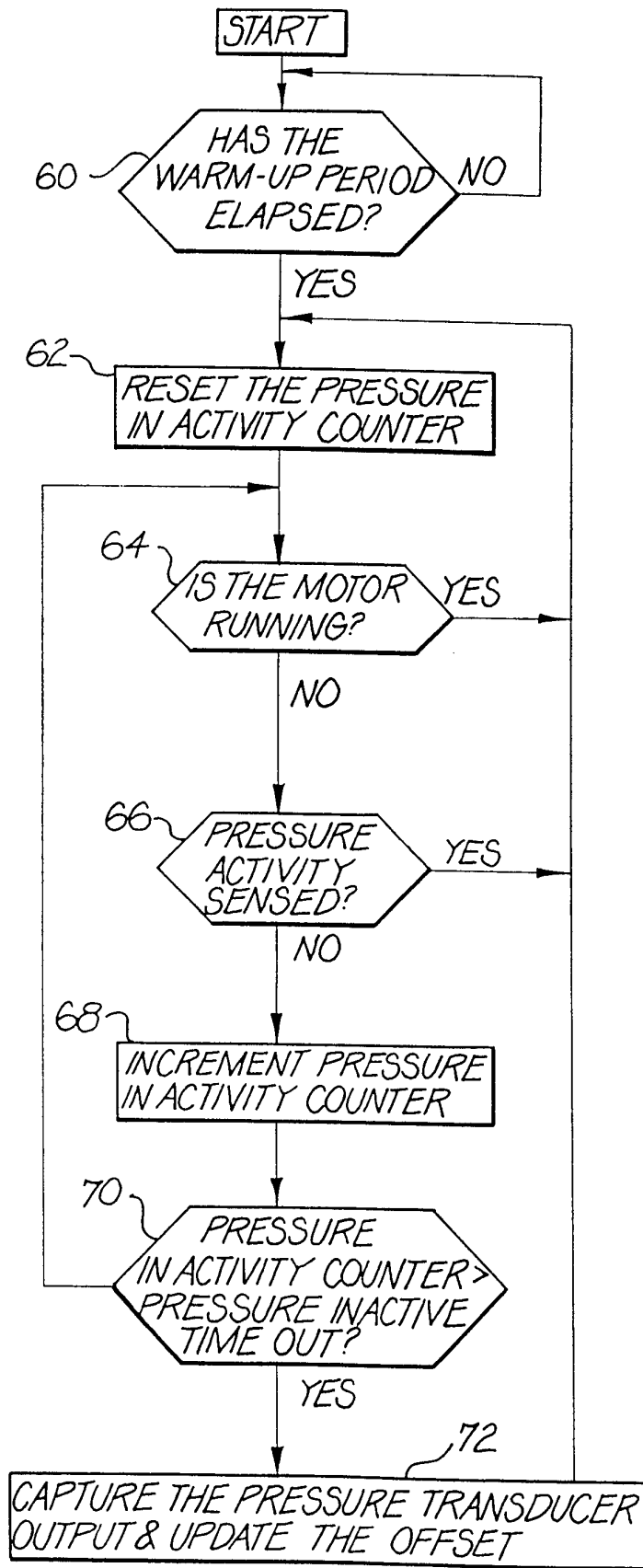


FIG. 3

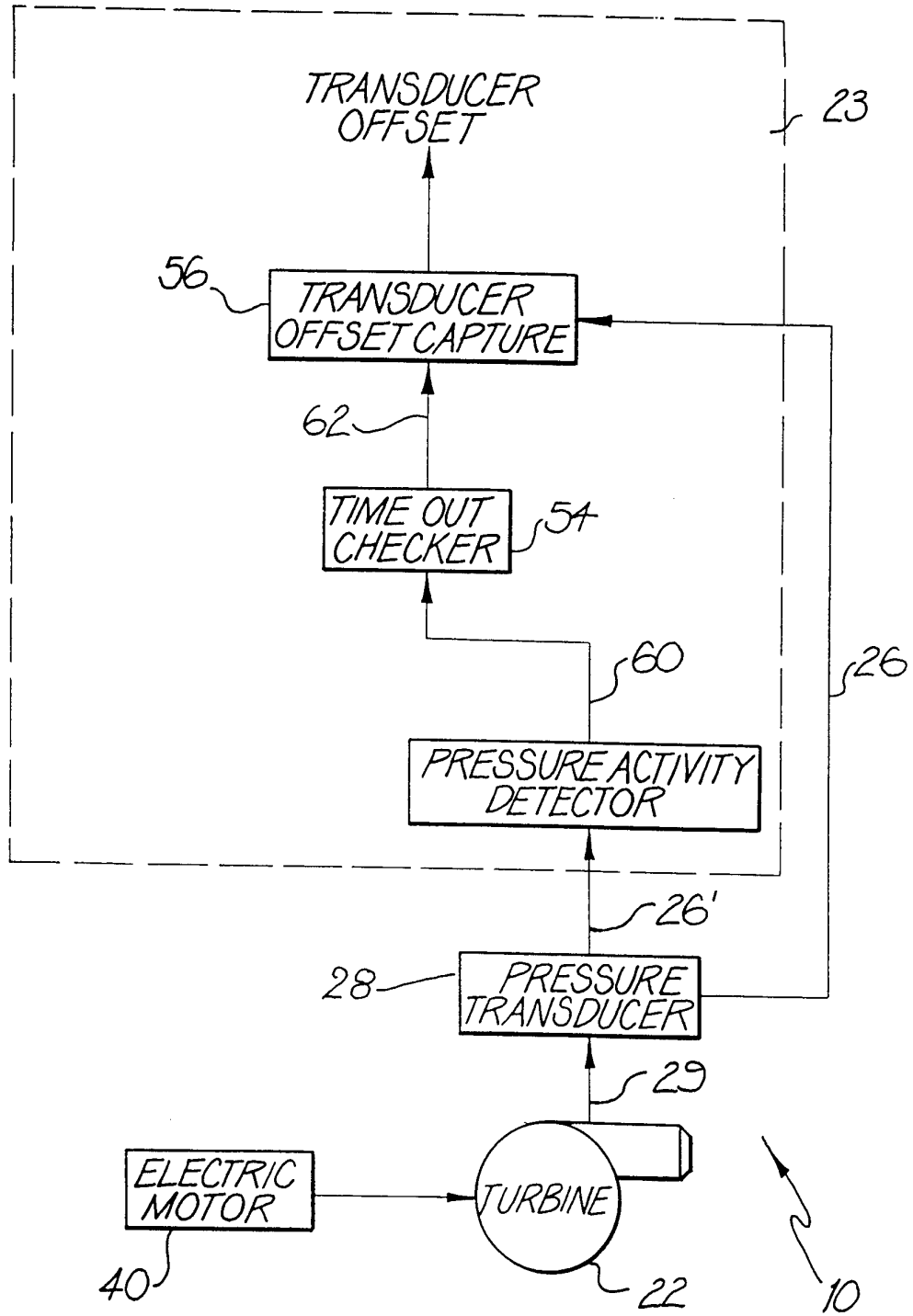


FIG. 4

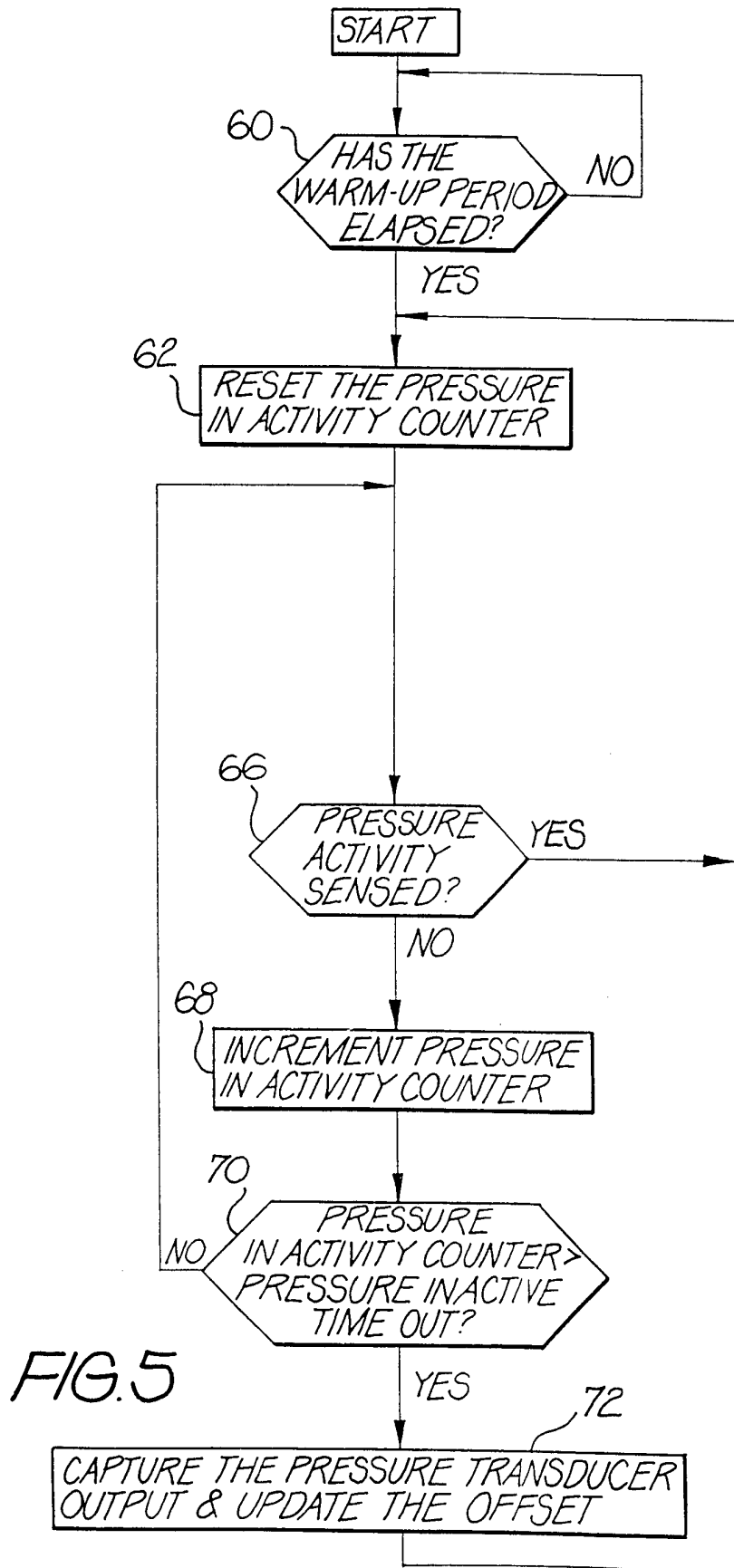


FIG. 5

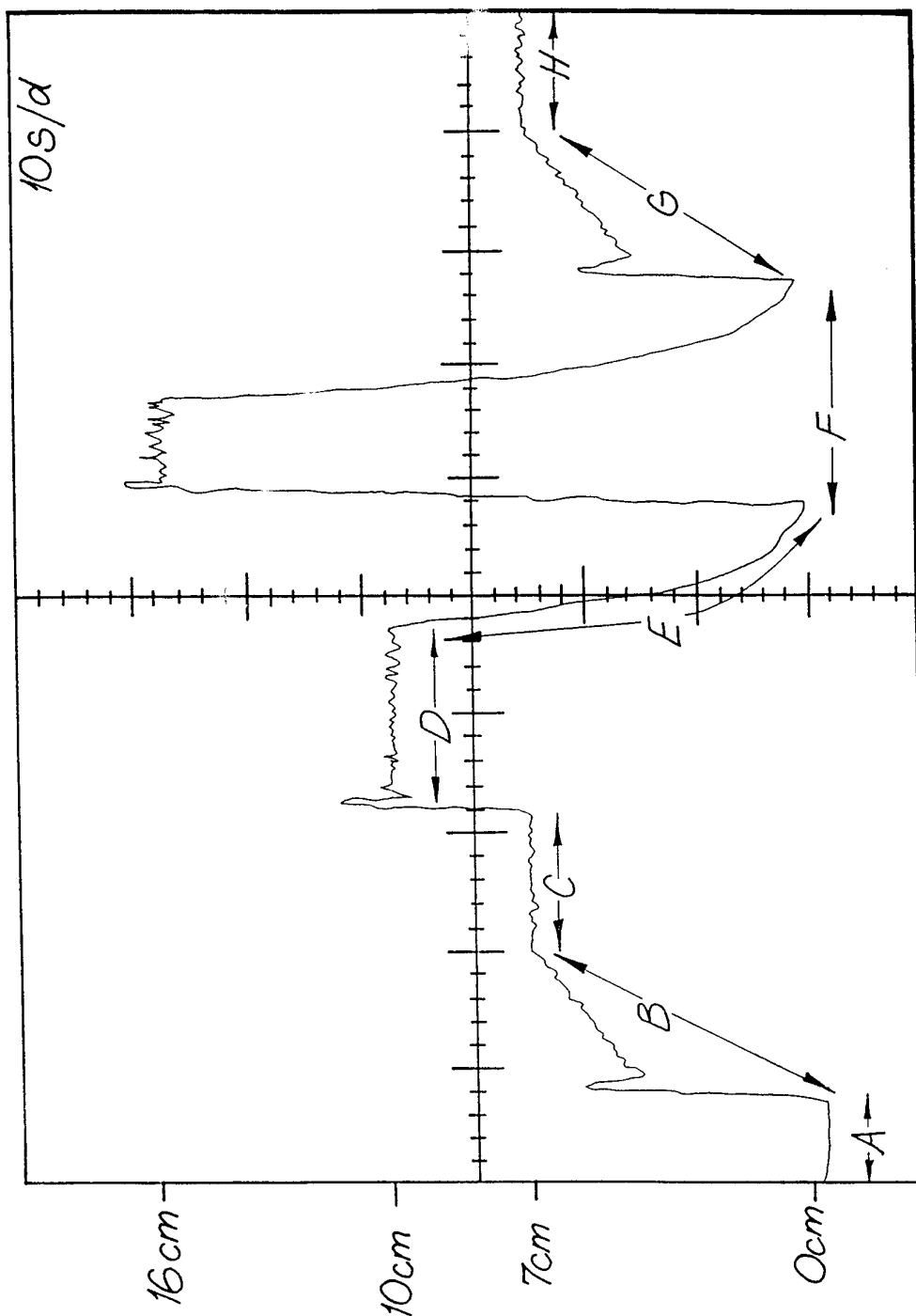


FIG.6

INTERNATIONAL SEARCH REPORT

International Application No.
PCT/AU 96/00413

A. CLASSIFICATION OF SUBJECT MATTER

Int Cl⁶: A61M 16/00, A62B 7/00 // G01F 25/00, G12B 13/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC A61B, A61H, A61M, G01F, G01L, G12B, G05D

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
AU IPC: A61B 5/08, A61H 31/00, A61M 16/00, A62B 7/00, G01F 25/00, G01L 27/00, G12B 13/00

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
DERWENT: calibrat, autocalibrat: pressure transduc: flow:
JAPIO

C. DOCUMENTS CONSIDERED TO BE RELEVANT


Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 3903785 A (HUGHES) 9 September 1975 column 1 lines 24-67, column 3 lines 1 to 63	1-16
X	US 4827922 A (CHAMPAIN et al) 9 May 1989 column 2 lines 29 to column 3 line 3, claims 4 to 7	1-16
X	GB 2254700 A (DRAGERWERK AKTIENGESELLSCHAFT) 14 October 1992 page 2 line 30 to page 4 line 3, page 5 line 21 to page 6 line 7	1-16

Further documents are listed in the continuation of Box C See patent family annex

* Special categories of cited documents:

"A"	document defining the general state of the art which is not considered to be of particular relevance	"T"	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"E"	earlier document but published on or after the international filing date	"X"	document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"L"	document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"Y"	document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"O"	document referring to an oral disclosure, use, exhibition or other means	"&"	document member of the same patent family
"P"	document published prior to the international filing date but later than the priority date claimed		

Date of the actual completion of the international search 9 August 1996	Date of mailing of the international search report 4 SEP 1996
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Name and mailing address of the ISA/AU AUSTRALIAN INDUSTRIAL PROPERTY ORGANISATION PO BOX 200 WODEN ACT 2606 AUSTRALIA Facsimile No.: (06) 285 3929	Authorized officer  MATTHEW FORWARD Telephone No.: (06) 283 2606
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INTERNATIONAL SEARCH REPORT

International Application No.

PCT/AU 96/00413

C (Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 4448058 A (JAFFE et al.) 15 May 1984 column 2 lines 5 to 68, column 3 lines 29-39 figure 1	1-16
Y	EP 425092 A1 (RESPIRONICS) 2 May 1991 column 3 lines 11-16, column 3 lines 34 to 58, column 5 lines 32 to 54, column 6 lines 27 to 33, column 10 lines 12 to column 11 line 23, figure 1.	1-16
Y	US 5134995 A (GRUENKE et al.) 4 August 1992 column 2 lines 51 to 68, column 3 lines 9 to 19, column 7, lines 45 to 88, figure 3	1-16
Y	Patent Abstracts of Japan, E 146, page 43, JP 54-104369 A (TOKYO SHIBAURA DENKI K.K.) 16 August 1979 Abstract	1-16
Y	5170798 A (RIKER) 15 December 1992 column 3 line 57 to column 4 line 2, claim 1	1-16

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No.

PCT/AU 96/00413

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report		Patent Family Member					
US	3903875						
US	4827922	EP	285470	FR	2611505	JP	063229063
GB	2254700	DE	4111965	FR	2675050	US	5253640
US	4448058						
EP	425092	AU	62221/90	AU	38508/93	AU	30678/95
		AU	30679/95	CA	2024477	EP	425092
		FI	904566	JP	3222963	US	5148802
		US	5239995	US	5433193	US	5313937
US	5134995	AU	59270/90	AU	33877/93	AU	48748/93
		AU	34471/95	EP	472664	US	5259373
		AU	82154/91	AU	40711/95	CA	2097502
		EP	563044	WO	9211054		
US	5170798	AU	29827/89	CA	1325460	EP	328415
		JP	1244736	US	5058601		
JP	54-104369						
							END OF ANNEX