



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

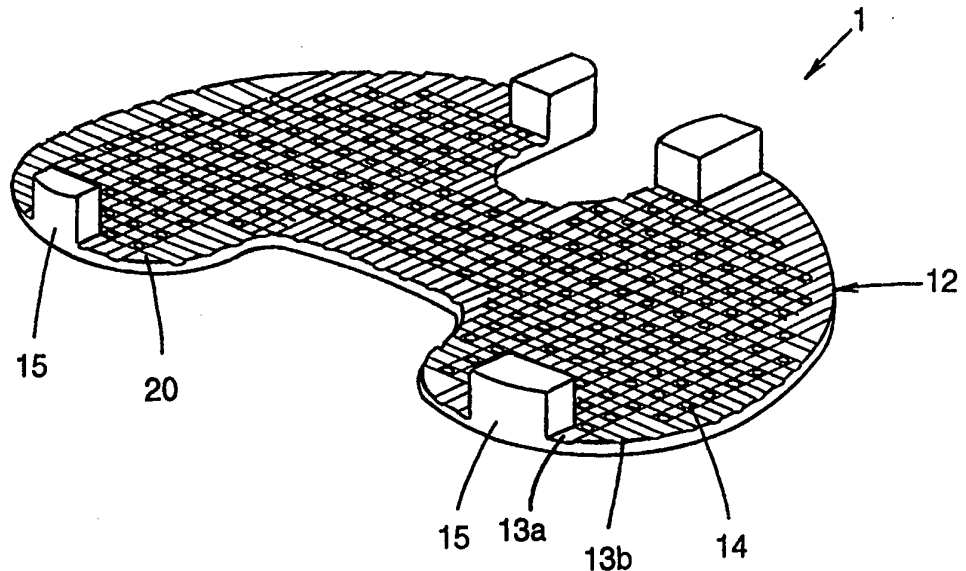
(51) International Patent Classification ⁶ : A61F 2/30	A1	(11) International Publication Number: WO 95/11639 (43) International Publication Date: 4 May 1995 (04.05.95)
<p>(21) International Application Number: PCT/IB94/00286</p> <p>(22) International Filing Date: 21 September 1994 (21.09.94)</p> <p>(30) Priority Data: 08/146,281 29 October 1993 (29.10.93) US</p> <p>(60) Parent Application or Grant (63) Related by Continuation US 08/146,281 (CON) Filed on 29 October 1993 (29.10.93)</p> <p>(71) Applicant (for all designated States except US): HOWMEDICA INC. [US/US]; 235 East 42nd Street, New York, NY 10017 (US).</p> <p>(72) Inventor; and (75) Inventor/Applicant (for US only): SCHWARTZ, Melvin, M. [US/US]; 616 Academy Drive, Point Pleasant, NJ 08742 (US).</p> <p>(74) Agents: SPIEGEL, Allen, J. et al.; Pfizer Inc., Patent Dept., 235 East 42nd Street, New York, NY 10017 (US).</p>	<p>(81) Designated States: AU, CA, DE (Utility model), JP, US, European patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).</p> <p>Published With international search report.</p>	

(54) Title: CAST BONE INGROWTH SURFACE

(57) Abstract

An article for use in preparing - and a process for preparing - a one-piece cast prosthetic bone implant (4) comprising a base (24), a porous ingrowth surface comprising a lattice element (33), comprising intersecting elongated connecting members (21 and 22) spaced from each other and from the base and spacing elements (23) to connect the base (24) and the lattice element (33), wherein the article comprises a pre-formed ceramic pattern (3) for the porous surface comprising a flat ceramic sheet (12a) comprising in a first surface thereof: (a) a plurality of intersecting semicircular grooves (13a', 13b');

(b) holes (14) at the intersections of the grooves; and (c) protrusions (15) from the first surface to aid alignment of the pattern in the meltable composition investment die (2); wherein the grooves (13a', 13b') are of such dimensions that when the article is placed in the investment die (2) they form cavities, with complementary grooves (13a'', 13b'') therein, corresponding to the connecting members (21, 22) of the lattice element (33).



FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AT	Austria	GB	United Kingdom	MR	Mauritania
AU	Australia	GE	Georgia	MW	Malawi
BB	Barbados	GN	Guinea	NE	Niger
BE	Belgium	GR	Greece	NL	Netherlands
BF	Burkina Faso	HU	Hungary	NO	Norway
BG	Bulgaria	IE	Ireland	NZ	New Zealand
BJ	Benin	IT	Italy	PL	Poland
BR	Brazil	JP	Japan	PT	Portugal
BY	Belarus	KE	Kenya	RO	Romania
CA	Canada	KG	Kyrgystan	RU	Russian Federation
CF	Central African Republic	KP	Democratic People's Republic of Korea	SD	Sudan
CG	Congo	KR	Republic of Korea	SE	Sweden
CH	Switzerland	KZ	Kazakhstan	SI	Slovenia
CI	Côte d'Ivoire	LI	Liechtenstein	SK	Slovakia
CM	Cameroon	LK	Sri Lanka	SN	Senegal
CN	China	LU	Luxembourg	TD	Chad
CS	Czechoslovakia	LV	Latvia	TG	Togo
CZ	Czech Republic	MC	Monaco	TJ	Tajikistan
DE	Germany	MD	Republic of Moldova	TT	Trinidad and Tobago
DK	Denmark	MG	Madagascar	UA	Ukraine
ES	Spain	ML	Mali	US	United States of America
FI	Finland	MN	Mongolia	UZ	Uzbekistan
FR	France			VN	Viet Nam
GA	Gabon				

-1-

5

CAST BONE INGROWTH SURFACE
BACKGROUND OF THE INVENTION

Field of the Invention

This invention relates to an integrally cast tissue ingrowth surface apparatus and a method for casting the same. More particularly, the invention relates to an integrally cast bone or tissue ingrowth surface in a cast metal orthopedic prosthesis.

Description of the Prior Art

Investment casting or the "lost wax process" has been used for over 50 years in the production of medical and dental implants. The process derives its name from the investment of wax or other suitable mold material and ceramics used to produce an expendable mold for casting metallic implants.

The investment casting process used to prepare orthopedic implants is common to the industry and is used to produce implants from Co-Cr-Mo (Vitallium® [Pfizer Hospital Products Group, Inc., New York, NY]) alloys as well as titanium alloys and stainless steels. Being well suited to the manufacture of the complex shapes typical of many implant designs, investment casting is used extensively to produce components for bone implants or total joint prostheses such as knees and hips.

These prostheses typically consist of metallic and polymeric components where the metallic components rest against bone on one side of the joint and bear against the polymeric component on the other. The bearing surfaces of a total joint have evolved in design to closely mimic the movement of the natural joint, while the bone contacting sides have evolved to assure improved fixation of the implanted prosthesis with the surrounding bone.

Until recently, total joint prostheses were designed for implantation with bone cement. For example, a polymethylmethacrylate (PMMA) grouting agent may be used to secure the prosthesis component against the surrounding bone. Implant surfaces contacting the cement were either cast smooth or with a two dimensional texture intended to improve fixation with the PMMA grout.

Recurrent loosening of these cemented implants, due to loss of support in underlying bone, lead to the development of prostheses with three dimensionally porous fixation surfaces which could be used without the PMMA bone cement. These prostheses, instead, rely on fixation via the ingrowth of bone or other connective tissue directly into the prosthesis surfaces, thereby anchoring the prosthesis to the bone.

-2-

These three dimensionally textured surfaces are created by bonding a suitable network of material, usually metal of the same composition as the implant, onto the implant's fixation surfaces to create a porous coating. The nature of the porosity present in the coating is generally a direct function of the materials and methods used to produce the coating.

Porous surfaces have been created by plasma spraying (United States Patent No. 3,605,123) of fine metallic particles, or by sintering a loosely packed coating of metallic particles (United States Patent No. 4,550,448, British Patent No. 1,316,809), or by diffusion bonding kinked fiber metal pads (United States Patent No. 3,906,550), or overlapping mesh (United States Patent No. 4,636,219).

In another concept, integrally formed ceramic filled porous areas are formed on the prosthesis. United States Patent No. 4,722,870 discloses a method for investment casting a composite implant which produces a porous metal structure filled with a ceramic (hydroxyapatite). However, this structure cannot be accurately controlled nor can it be spaced a predetermined distance above the outer surface of the implant.

Other United States Patents describe mesh surfaces welded to the implant. Such a mesh is shown in United States Patent No. 3,905,777 to Lacroix, United States Patent No. 4,089,071 to Kalnberz et al., United States Patent No. 4,261,063 to Blanquaert and United States Patent No. 4,636,219 to Pratt et al. None of these surfaces are integrally cast with the prosthesis.

Each of the aforementioned methods for producing a porous ingrowth surface entails applying a porous network onto the surface of a metallic implant and bonding that network through the application of heat. Plasma spraying employs super heated gases to melt the metal particles to be sprayed. Sintering develops interparticle bonds in a porous coating by exposing the coating and implant metal to temperatures approaching their melting point, while diffusion bonding employs heat and pressure to promote atomic diffusion at the coating implant interface.

Each of these methods has its limitations. Plasma spraying cannot be adequately controlled to achieve a uniform interconnected pore structure in the coating. The temperatures required for sintering have a deleterious effect on the implant material's strength and diffusion bonding develops variations in pore structure and bond quality due to variations in pressure distribution during the coating process. Each of

-3-

the processes is limited in its achievable pore size by the loss in coating strength which occurs as coating porosity increases.

Particulate porous coatings are also inherently accompanied by a dramatic increase in surface area of metal exposed to body fluids thereby increasing, proportionally, the corrosion products which are released after implantation.

European Patent Application No. 0 230 006 describes a bone implant with a netlike surface covering which contains a large number of perforations for the ingrowth of bony substance and consists of at least two assemblages of elongated crisscrossing elements. To provide satisfactory spaces with precisely predeterminable dimension for newly formed bone tissue, the elongated elements run parallel to the surface of the implant core that lies beneath them, with the attachment of the elements to the core material and maintenance of the distance from the core being ensured by projections.

Clinical reports exist of metal particles becoming loose from bonded coatings or fiber pads becoming detached on revision surgery. Furthermore, bonded coatings inherently develop stress concentrating surface notches at the coating - substrate interface which limit the locations a porous coating can be placed due to strength considerations. By their very nature, bonded coatings require the use of a secondary manufacturing process to affix the coating to the implant surfaces. These processes increase manufacturing costs through added labor, materials, tooling and fixturing.

United States Patent No. 5,108,435 describes an orthopedic implant comprising a base and a porous surface wherein the base and surface are formed in a one-step casting process. The porous surface is uniformly spaced from the surface of the base.

SUMMARY OF THE INVENTION

This invention provides a one step process for forming a porous fixation surface (hereafter porous surface) on an implant, for purposes of improved implant fixation to the underlying bone, which is an integral part of the implant. The porous surface is produced by casting a three dimensional grid-like, or lattice structure directly, onto the implant surface.

A further object is to provide a one step process for creating a porous surface on an implant which does not require thermal processing, which may be detrimental to the substrate materials mechanical properties, and does not involve the expense of a secondary coating process.

-4-

Another object is to allow the porous surface on an implant to be precisely controlled relative to pore shape, pore size, pore size distribution, substrate bonding and coating stress concentrations.

It is yet another object of the invention to allow the pore sizes and shapes to vary and the spacing of the porous surface to be non-uniform.

These and related objects are achieved in the present invention by an implant having a cast metal base member having a first surface designed to rest against a bone after implantation and a tissue ingrowth surface in the form of a cast metal lattice element, composed of a grid-like element, spaced from the base member second surface, and integrally cast with the base member, from the same metal, over at least a part of the second surface thereof. The metal utilized may be "Vitallium", titanium alloy or other suitable biocompatible metallic alloy.

An investment casting technique, wherein a meltable material is coated with a ceramic casting shell, may be utilized to cast the tissue ingrowth porous surface and the base member of the metal orthopedic implant in a single step. As is well known, the meltable material, such as wax, has a melting point lower than the ceramic material. A pattern for the porous surface is formed from the ceramic material, e. g., by injection molding, and inserted in the meltable material die corresponding to the implant. Meltable material is then added to the die partially encapsulating the ceramic pattern and forming a tri-axial matrix network. The combined meltable material ceramic pattern is coated with a ceramic slurry to form a casting shell in the manner well known to the art. The meltable material is then removed from the casting shell by heating. As is well known, the empty casting shell is filled with molten metal and allowed to cool, thereby forming a one piece casting in the form of the pattern corresponding to the orthopedic implant with the lattice integrally cast therewith. Since the preformed ceramic pattern was designed to be semi-exposed the process results in an implant having a three-dimensional porous fixation surface as an integral part of the cast orthopedic product. While wax is preferably used as the meltable material other materials, such as polystyrene, may also be used. The depth of the cavities in the ceramic pattern may be varied to obtain various spacings of the porous surface from the implant.

The process enhances productivity by combining the meltable material injection operations of forming the implant base element and porous fixation surface into one step. This also eliminates any need for additional assembly or joining operations. The

-6-

Figure 6A is schematic sectional view of a meltable casting of an orthopedic implant comprising the base element and porous fixation surface covered by a casting shell after investment with a meltable material and removal from the meltable material die and coating with a ceramic shell.

5 Figure 6B is schematic sectional view of the casting and ceramic shell of Figure 6A after removal of the meltable material or formation by the DSPC method.

Figure 6C is a view of Figure 6B after molten base metal has been introduced into the ceramic shell of Figure 6B.

10 Figure 6D is schematic sectional view of the integrally cast orthopedic implant and lattice element of the present invention.

Figure 7 is a partial cross-sectional view of a femoral component of a total hip prosthesis having the porous tissue ingrowth surface in the form of the lattice element integrally cast on the outer surface thereof.

15 Figure 8 is a schematic sectional view of a second embodiment of the integrally cast orthopedic implant and lattice element of the present invention wherein the porous surface is non-uniformly spaced from the implant.

DETAILED DESCRIPTION OF THE INVENTION

Referring to Figures 1-4 and 7 there is shown a preformed ceramic pattern 1, of the present invention, in the form of a lattice element, for a porous ingrowth surface of an orthopedic implant, such as that for a femoral which is shown in Figure 7. Pattern 1 may be prepared by injection molding in any known manner. Pattern 1 as shown in Figure 1-4 would be useful for a tibial or knee fibial implant. The shape of the pattern may be changed to conform to the shape of implants for other indications such as hip or femoral knee components.

25 Pattern 1 consists of a flat ceramic sheet 12 comprising transverse, generally perpendicular, grooves 13a and 13b, intersecting at holes 14, corresponding to connectors 23' of the implant in Figure 7, in a first surface 16 of said sheet, which space connectors 13a' and 13b' from the base 24' of the implant. In addition, the pattern comprises projections 15 perpendicular to surface 16, for aligning the pattern in a meltable material investment mold such as is shown schematically in Figure 5B and designated with the numeral 2.

30 A preferred ceramic pattern for a portion of a porous surface is shown schematically in Figure 5A and designated 3. The pattern, which may be formed by

-7-

known methods, such as injection molding, comprises a flat ceramic sheet 12a comprising generally perpendicular grooves 13a' and 13b' which intersected holes 14a, through the ceramic sheet 12a. The insert also comprises protrusions 15, perpendicular to the surface of the ceramic sheet 12 which aid in aligning the insert in a meltable composition die such as is shown schematically in Figure 5B and designated 2. The die comprises two releaseably joinable sections, designated 2a and 2b. Section 2a comprises intersecting grooves 13a'' and 13b'' which, upon emplacement of the pattern 3 in the die form elongated cavities corresponding to the connectors 21 and 22 of implant 4 in Figure 6D. The second section 2b comprises a cavity 16 a portion 31 of which, that is left over after emplacement of the pattern 3 therein as shown in Figure 5C, corresponds to the base 24 of the implant.

The practice of the invention is best described with reference to Figures 5A-6D, wherein the porous surface pattern 3, shown in Figure 5A, is inserted into section 26 of meltable composition die 2. The meltable material 20 is injected into die 2 through port 18 to fill the cavities 13 formed from grooves 13a', 13b', 13a'' and 13b'', the holes 14 of the ceramic pattern 3 and the cavity 16 of the die. After the cavities comprising grooves 13a', 13b', 13a'' and 13b'', holes 14 and cavity 31 have been filled with the meltable material 20 they form a meltable casting of the implant. The casting is removed from the die and is coated with a colloidal silica binder, to form a shell 19 as shown in Figure 6A. The colloidal silica is selected from the group including refractory powders of zirconia, alumina and silica and is applied to the meltable casting as a slurry. The first coat of the slurry used to form the shell in the investment casting process is critical. A preferred slurry for this first coat is a colloidal silica binder (such as Du Pont's 30% colloidal binder) base with refractory zirconia and silica flours. The viscosity can be varied by adding more or less binder. The dip pattern must be designed to make sure that the one-piece casting is completely and evenly coated. The casting must be vibrated while draining, with air lightly blown over the lattice pattern to break up any air bubbles which might prevent the slurry from bridging the grid openings. With care, it has been found that this technique can be used to produce grid openings of about 50 mm (0.02 inches) and above. With the use of the injection molding process for the meltable material, various pattern shapes, such as square, rectangular or triangular, may be used for the ceramic tissue ingrowth lattice surfaces. With this process, furthermore, the shapes and sizes can be accurately controlled.

-8-

Thus, various pattern shapes can be fabricated to fit specific implant designs. Furthermore, the potential variability of pore spacing would allow for the use of bone inductive coatings or fillers such as hydroxyapatite to facilitate tissue or bone ingrowth as well as more precise engineering and control of pore structures as required for
5 improved osseo integration or vascularization.

After the initial coat is allowed to dry, the process continues with, additional slurry coats being applied, in the well known manner, as desired, to complete forming the ceramic shell 19 on the meltable material pattern for the porous surface and implant, as shown in Figure 6A. The meltable casting, comprising the intersecting is
10 then removed from the shell by heating in a well known manner. This results in a void being formed within ceramic shell 19, as shown in Figure 6B corresponding to connectors 21a and 22a, spacers 23a of the surface and base 24a, of the implant 4 shown in Figure 6D. A molten metal, such as Vitallium or a tantalum alloy or titanium, is introduced into the void, as shown in Figure. 6C, and allowed to cool. Of course, it
15 is well known that in order to cast titanium, special foundry practices must be followed. Under those circumstances, cast ingrowth surface of the present invention, comprising titanium, can be produced.

Removal of shell 19, integral one-piece metal casting of an implant 4, comprising a base 24, and a porous fixation surface comprising a lattice element comprising
20 intereseting connectors 21 and 22 connectors 23 to space the lattice element from the base 24 and pores 26 as shown in Figure 6D.

Referring to Figure 7, it can be seen that the integral cast lattice element forming a tissue ingrowth surface comprising connectors 21' and 22', can be easily produced on the outside of a femoral component of a hip prosthesis. This is accomplished by
25 producing a spherical preformed ceramic core that replicates the outer surface 24'' of the hip prosthesis utilizing a meltable material formulation, such as wax or polystyrene, which is suitably flexible and can be wrapped around the outer surface of a hip prosthesis. Such a wax is Yates JW-2® (Yates Manufacturing Co., Chicago, IL 60608) wax.

30 Alternatively, the mold of Figure 6B may be prepared by the process of Direct Shell Production Casting™ (Soligen, Inc., Northridge, CA.)

In a second embodiment of the invention the porous surface of the implant is not uniformly spaced from the base. As shown, in Figure 8, for an implant designated

by the numeral 5, alternate rows of spacers 28 and 29, in the implant have different heights thus resulting in differing displacements of the connectors 27 from the base 29 and varying forms of the pores 30.

In a third embodiment, now shown, alternate spacers, rather than rows of 5 spacers, may have varying heights.

While several examples of the present invention have been described, it is obvious that many changes and modifications may be made thereunto, without departing from the spirit and scope of the invention.

-10-

CLAIMS

1. An article for use in preparing a one-piece cast metal prosthetic bone implant (4) comprising a base (24), a porous ingrowth surface comprising a lattice element (33), comprising intersecting elongated connecting members (21 and 22) spaced from each other and from said base and spacing elements (23) to connect the base (24) and the lattice element (33), wherein said article comprises a preformed ceramic pattern (3) for said porous surface comprising a flat ceramic sheet (12a) comprising in a first surface thereof
- 5
- a) a plurality of intersecting semicircular grooves (13a', 13b');
b) holes (14) at the intersections of said grooves; and
c) protrusions (15) from said first surface to aid alignment of the pattern in the meltable composition investment die (2) by insertion into complementary cavities (15') thereof;
- 10
- wherein said grooves (13a', 13b') are of such dimensions that when the article is placed in said investment die (2) they form cavities, with complementary grooves (13a", 13b") grooves therein, corresponding to the connecting members (21, 22) of the lattice element (33).
- 15
2. The article of claim 1 wherein said intersecting grooves are not parallel.
3. The article of claim 1 wherein said holes (14) are of equal length.
20 4. The article of claim 1 wherein said holes (14) are of unequal length.
5. The article of claim 1 wherein said meltable composition is a wax.
6. A process for preparing a one-piece cast metal prosthetic bone implant (4) comprising (24), a porous ingrowth surface comprising a lattice element (33), comprising intersecting elongated connecting members (21 and 22) spaced from each other and from said base and spacing elements (23) to connect the base (24) and the lattice element (33), which comprises the steps of
- 25
- a) adding molten metal to a ceramic mold for said implant wherein said mold comprises
- 30
- 1) a ceramic shell (19);
2) a preformed ceramic pattern (3), within said shell (19), for said porous surface comprising a flat ceramic sheet (12a) comprising in a first surface thereof

-11-

- i) a plurality of intersecting semicircular grooves (13a', 13b');
- ii) holes (14) at the intersections of said grooves corresponding to the spacers (23);
- 5 3) a plurality of cavities, formed from the above grooves (13a', 13b') and complementary grooves (13a", 13b"), in a meltable composition investment die (2), corresponding to the intersecting members (21, 22) of the lattice element (33);
- 4) a cavity (34) corresponding to the base (24) of the implant
- 10 (4); and
- b) removing the shell (19) to leave the casting of the implant containing the ceramic pattern (3); and
- c) removing the ceramic pattern (3) from the implant (4).
7. The process of claim 6 wherein the ceramic pattern (3) is removed by
- 15 leaching with a base.
8. The process of claim 6 wherein the mold is made by the meltable composition investment method.
9. The process as set forth in claim 6 wherein said metal is a cobalt-chrome alloy.
- 20 10. The process as set forth in claim 6 wherein said metal is cobalt-chrome.
11. The process as set forth in claim 6 wherein said connecting elements (21, 22) and spacers (23) define openings (26) between the lattice element (33) and the base (24) of the implant (4) to allow for tissue ingrowth.
12. The process as set forth in claim 6 wherein said connecting elements
- 25 (21, 22) and spacers (23) define openings (26) between the lattice element (33) and the base (24) of the implant (4) to allow for the introduction of bone cement.
13. The process of claim 6 wherein the ceramic mold comprising the cavity (34), corresponding to the base (24) of the implant, and the ceramic pattern (3), for the lattice element (33) and spacers (23), is prepared by
- 30 a) inserting the preformed ceramic pattern (3) comprising a flat ceramic sheet (12a) comprising in a first surface thereof
- b) a plurality of intersecting semicircular grooves (13a', 13b');
- c) holes (14) at the intersections of said grooves; and

-12-

d) protrusions (15) from said first surface to aid alignment of the pattern in the meltable composition investment die (2) by insertion into complementary cavities (15') thereof;

wherein said grooves (13a', 13b') are of such dimensions that when the article
5 is placed in said investment die (2) they form cavities, with complementary grooves (13a", 13b") grooves therein, corresponding to the connecting members (21, 22) of the lattice element (33) into the die (2) and injecting a material, meltable below the melting temperature of the ceramic, in its molten state into, and then cooling, the die to form a one-piece pattern for the implant (4).

10 c) coating said one-piece pattern with a ceramic coating to form a shell (19); and

d) heating the coated pattern and removing the meltable material to form the ceramic mole containing the hollow base pattern (34), and ceramic pattern for the lattice element (33) and spacers (23).

15 14. The process of claim 13 wherein said meltable material is a wax or thermoplastic polymer.

15. The process of claim 14 wherein said meltable material is a wax.

16. The process of claim 14 wherein said meltable material is a polystyrene.

17. The process of claim 6 wherein said ceramic pattern (3) comprises a
20 ceramic material selected from fused silica and alumina.

18. The process of claim 17 wherein said ceramic material is fused silica.

19. The process of claim 6 wherein said metal is selected from Vitallium, titanium, tantalum and alloys thereof.

20. The process of claim 19 wherein said metal is Vitallium.

25 21. The process of claim 19 wherein said metal is titanium or an alloy thereof.

22. The process of claim 19 wherein said metal is tantalum or an alloy thereof.

23. The process of claim 6 wherein said mold is prepared by the steps of

30 a) creating the design for the mold on a computer;

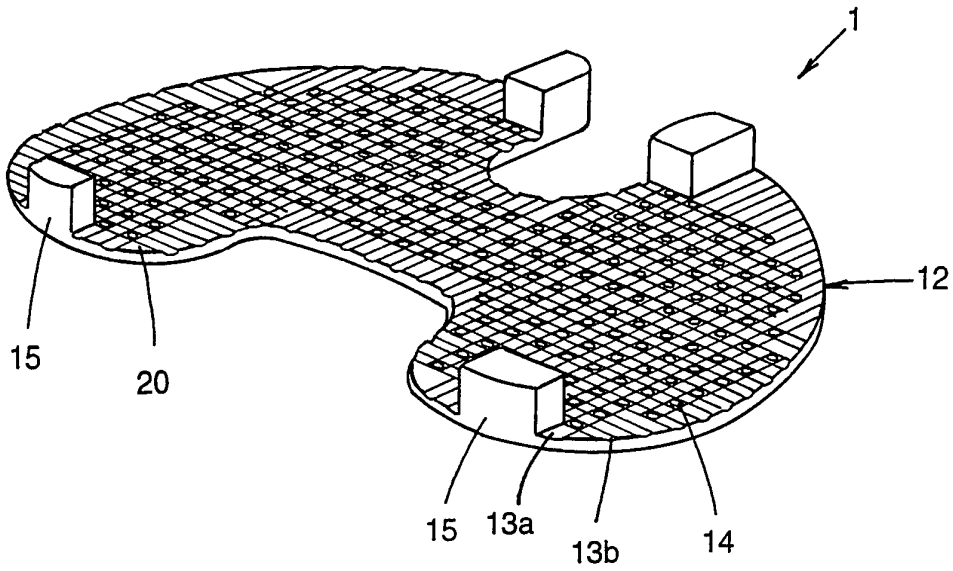
b) converting the design into a casting shell containing the patterns of the base member (24), spacers (27) and connecting elements (21, 22) of the lattice element (33); and

-13-

c) forming the shell and container, under computer control, one layer at a time by spreading ceramic powder, then printing it with a liquid binder and removing excess powder.

24. A one-piece cast metal prosthetic bone implant (5) comprising a base
5 (24), a porous ingrowth surface comprising a lattice element comprising intersecting elongated connecting members (27, 32) spaced from each other and from said base and spacing elements (28, 29) to connect the base (24) and the connecting members (27, 32) wherein the spacing elements (28, 29) are of unequal lengths.

FIG. 1



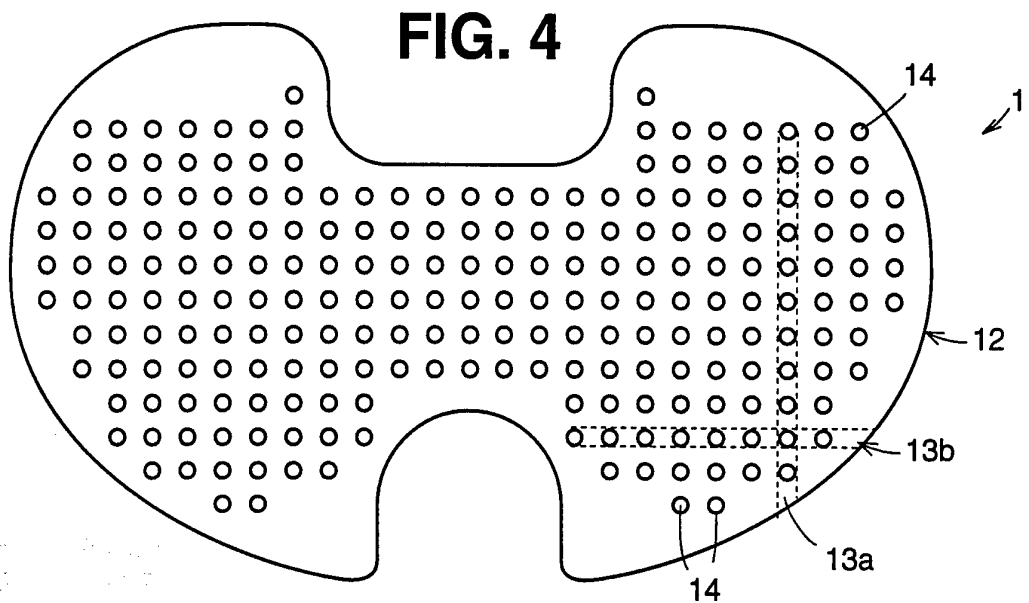
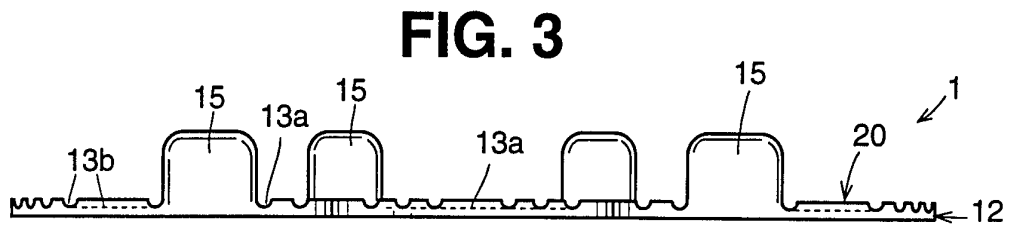
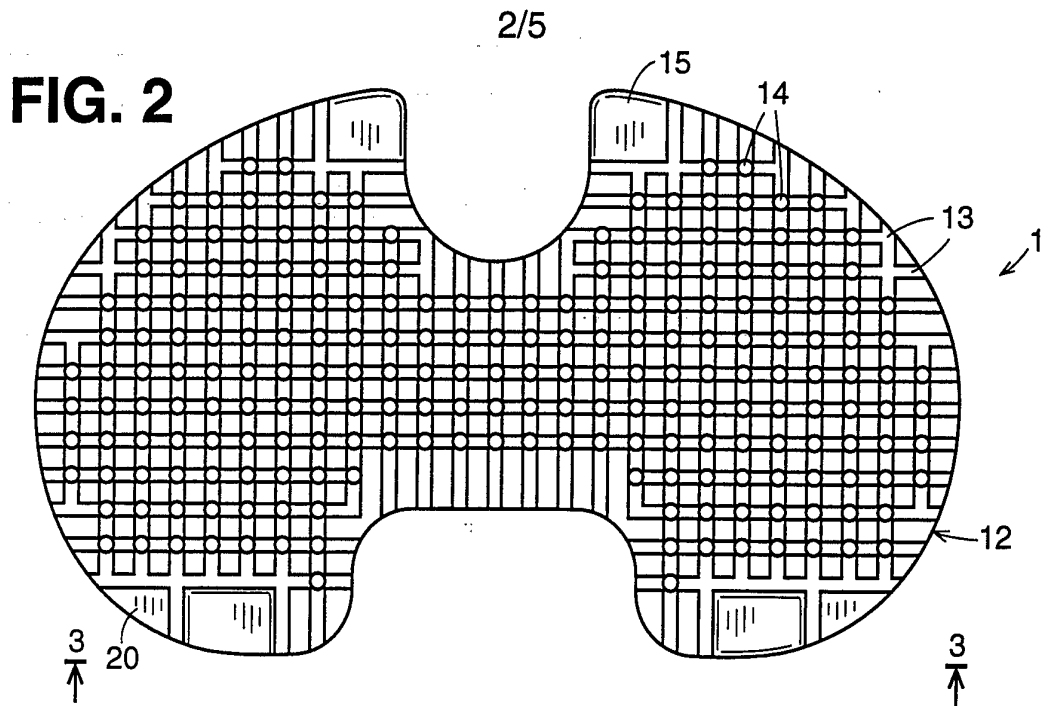


FIG. 5A

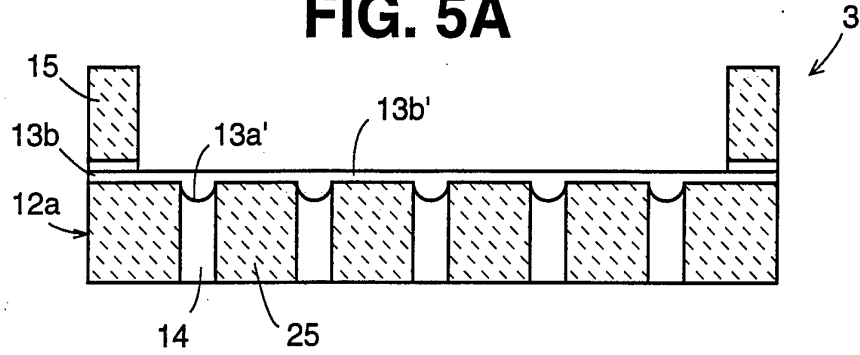


FIG. 5B

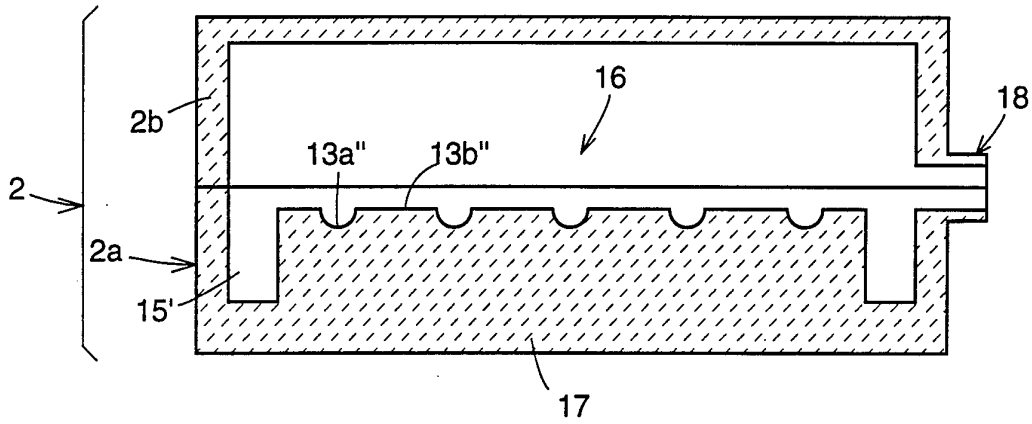


FIG. 5C

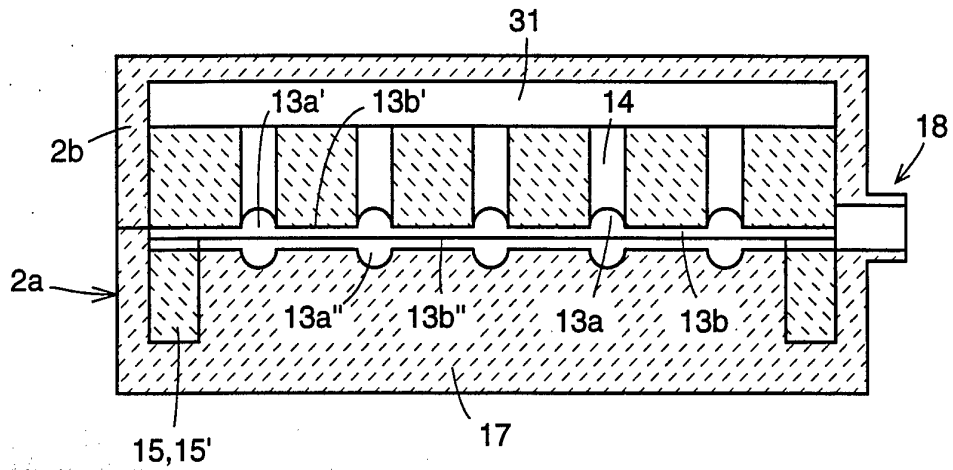


FIG. 6A

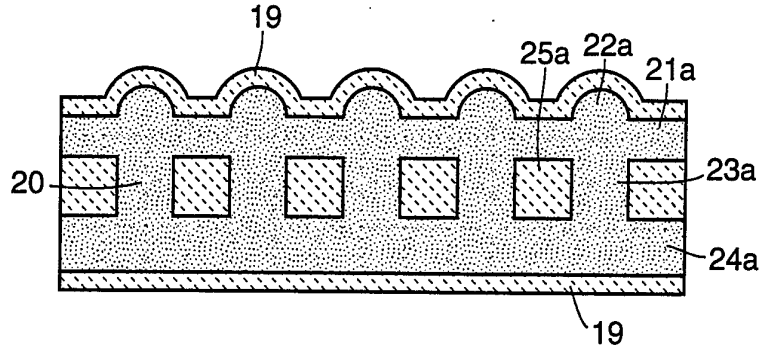


FIG. 6B

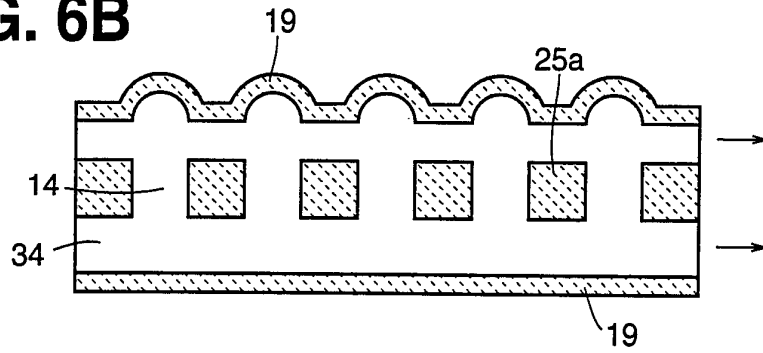


FIG. 6C

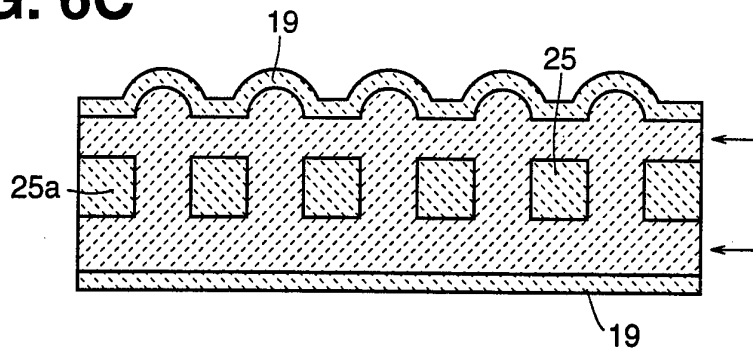


FIG. 6D

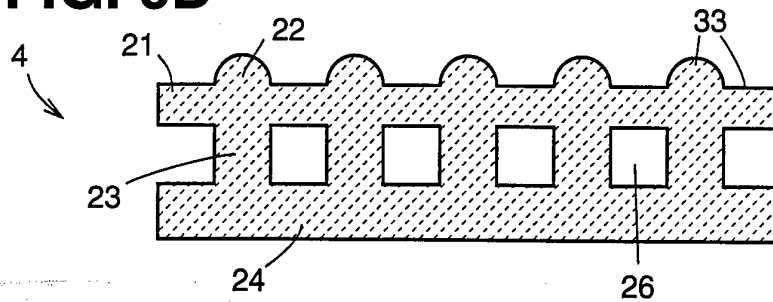


FIG. 7

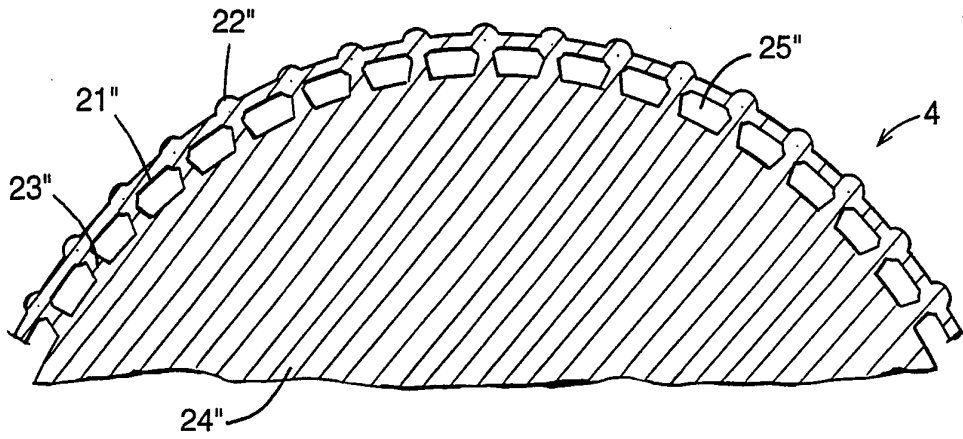
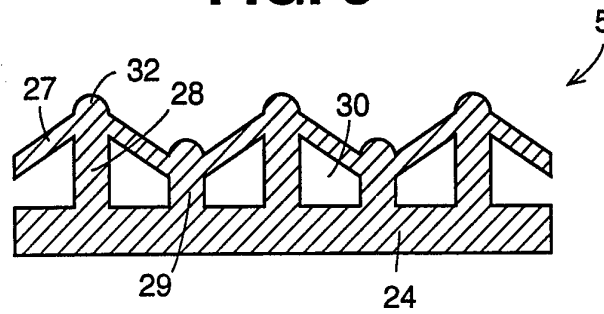


FIG. 8



INTERNATIONAL SEARCH REPORT

International Application No
PCT/IB 94/00286

A. CLASSIFICATION OF SUBJECT MATTER		
A 61 F 2/30		
According to International Patent Classification (IPC) or to both national classification and IPC ⁶		
B. FIELDS SEARCHED		
Minimum documentation searched (classification system followed by classification symbols)		
A 61 F		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practical, search terms used)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	DE, A, 3 715 000 (KRUPP) 17 November 1988 (17.11.88), claims 1,6,7; fig. 1. --	1,24
A	DE, A, 3 844 155 (MECRON) 28 June 1990 (28.06.90), claims 1,2; fig. 1,2. --	1,19, 21
A	DE, A, 3 923 418 (MIEHLKE) 12 July 1989 (12.07.89), column 4, lines 17-31; fig. 1,2,2a. --	1,24
A	EP, A, 0 255 797 (MECRON) 10 February 1988 (10.02.88),	6,23
<input checked="" type="checkbox"/> Further documents are listed in the continuation of box C. <input type="checkbox"/> Patent family members are listed in annex.		
* Special categories of cited documents :		
"A" document defining the general state of the art which is not considered to be of particular relevance "E" earlier document but published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. "&" document member of the same patent family		
Date of the actual completion of the international search 22 November 1994		Date of mailing of the international search report 14.12.94
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+ 31-70) 340-2040, Tx. 31 651 epo nl, Fax (+ 31-70) 340-3016		Authorized officer MIHATSEK e.h.

INTERNATIONAL SEARCH REPORT

-2-

International Application No
PCT/IB 94/00286

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
	the whole document. -----	

ANHANG

zum internationalen Recherchenbericht über die internationale Patentanmeldung Nr.

ANNEX

to the International Search Report to the International Patent Application No.

ANNEXE

au rapport de recherche international relatif à la demande de brevet international n°

PCT/IB 94/00286 SAE 96151

In diesem Anhang sind die Mitglieder der Patentfamilien der in obengenannten internationalen Recherchenbericht angeführten Patentdokumente angegeben. Diese Angaben dienen nur zur Unterrichtung und erfolgen ohne Gewähr.

This Annex lists the patent family members relating to the patent documents cited in the above-mentioned international search report. The Office is in no way liable for these particulars which are given merely for the purpose of information.

La présente annexe indique les membres de la famille de brevets relatifs aux documents de brevets cités dans le rapport de recherche international visée ci-dessus. Les renseignements fournis sont donnés à titre indicatif et n'engagent pas la responsabilité de l'Office.

In Recherchenbericht angeführtes Patentdokument Patent document cited in search report Document de brevet cité dans le rapport de recherche	Datum der Veröffentlichung Publication date Date de publication	Mitglied(er) der Patentfamilie Patent family member(s) Membre(s) de la famille de brevets	Datum der Veröffentlichung Publication date Date de publication
DE A1 3715000	17-11-88	DE C2 3715000 EP A1 289922 EP B1 289922 US A 4904262	20-04-89 09-11-88 19-06-91 27-02-90
DE A1 3844155	28-06-90	AT E 112952 CA AA 2006595 DE C2 3844155 DE C0 58908535 EP A2 375600 EP A3 375600 EP B1 375600 JP A2 2246970 US A 5015817	15-11-94 23-06-90 27-01-94 24-11-94 27-06-90 17-04-91 19-10-94 02-10-90 14-05-91
DE A1 3923418	31-01-91	keine - none - rien	
EP A1 255797	10-02-88	DE A1 3626549 DE C0 3763134 EP B1 255797	11-02-88 19-07-90 13-06-90