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# DESCRIPTION

## BACKGROUND OF THE INVENTION

### 1. Field of the Invention

**[0001]** The present invention relates to a biopsy device for obtaining tissue samples from human or animal tissue. The invention is particularly, but not exclusively, aimed at percutaneous biopsy, in which it is desirable to gain access to suspect tissue mass in a minimally invasive manner. The invention relates to a biopsy device that is optimized for the sampling of tissues that are resilient and difficult to cut using conventional approaches. Furthermore, a biopsy device is disclosed that is optimized to deliver the highest possible tissue yield.

### 2. Description of the Related Art

**[0002]** For diagnostic purposes it may be desirable to obtain a tissue sample of a human or animal body for cytological or histological in vitro examination. The tissue sample can be examined for specific qualities based on which a diagnosis can be made and therapy can be administered. For the harvesting of tissue samples, several approaches exist. The conventional open biopsy is increasingly being replaced by less-invasive biopsy methods, and especially the field of breast biopsy has seen rapid development of novel biopsy device types that reduce the invasiveness of the tissue sampling procedure.

**[0003]** In the percutaneous technique, a needle is used to gain access to the suspect tissue mass in a less invasive fashion. This needle may be hollow, permitting the aspiration of single cells and tissue fragments into a lumen by application of a vacuum (aspiration biopsy). Alternatively, larger tissue cores may be harvested by means of a needle containing an inner movable trocar with a notch formed to receive tissue cores, and an outer, slidable cutting cannula with a sharpened distal end used to sever these cores from the surrounding tissue (core needle biopsy). By advancing the inner trocar into a suspect lesion and subsequently advance the outer slidable cannula to cover the notch completely, a tissue sample may be severed and held in the notch. The needle may then be retracted from the body of the patient, and the tissue sample may be collected and stored for further analysis.

**[0004]** Several parameters define whether a tissue sample is useful for analysis, and one of the more important is the sample size. Core needles, while representing a less-invasive approach to tissue sampling, are often incapable of delivering samples of an adequate size for reliable diagnosis. Using vacuum to engage and draw tissue towards the sample notch can significantly increase tissue sample sizes for a given biopsy needle diameter thereby improving

diagnostic accuracy. Another well-known technique to increase sample size is to harvest multiple samples in order to obtain sufficient tissue for a reliable diagnosis. Instead of multiple insertions biopsy systems have been developed that enable the extraction of multiple samples with a single biopsy device insertion, the so called SIMS biopsy devices: "Single Insertion - Multiple Samples". These devices are typically vacuum assisted and may include a tissue-collecting portion that can be moved from an advanced position at the sampling site to a retracted position where the tissue sample may be collected. Exemplary SIMS biopsy devices are disclosed in prior art documents WO 2006/005342, WO 2006/005343, WO 2006/005344 and WO 2006/005345 employing a spring-loaded linear cutting cannula.

**[0005]** EP 0 895 752 A1 discloses a semi-automatic cardiac tissue removal device for obtaining biopsy samples and/or creating revascularization pathways in the myocardium of the heart. The device mechanically cuts the pathways using a hand piece with a cutting tip assembly having a hollow needle with an angled, sharpened edge rotatable mounted around a separately advanceable stylet. The stylet defines a piercer to spread the myocardium prior to insertion of the needle and to allow creation of a pathway only within the myocardium. The stylet further defines a plug at the cutting edge of the needle to finish the cutting cleanly and to plug the hollow needle thereby forming a closed chamber for excised tissue. A single button on the left or right handed hand piece actuates movement of the stylet into the myocardium, movement of the needle into the path produced by the piercer, and rotation of the needle to cut tissue.

#### SUMMARY OF THE INVENTION

**[0006]** In a first aspect of the present invention, there is disclosed a disposable unit for a biopsy device according to claim 1.

**[0007]** The present disclosure relates to a biopsy device for harvesting at least one tissue sample from a suspect tissue mass in a body of a living being, comprising a cutting cannula that is hollow, an inner member comprising a sharpened distal tip configured to be introduced into the body and a sample notch for receiving the at least one severed tissue sample, the inner member receivable in the cutting cannula, and a cutting mechanism configured for causing the cutting cannula to be longitudinally displaced in a distal direction from a first position at the proximal end of the sample notch exposing the sample notch, to a second position at the distal end of the sample notch, so as to sever said tissue sample from remaining body tissue at the harvesting site.

**[0008]** The inner member may be a rigid and/or rotatable toothed rack that is longitudinally displaceable in the cutting cannula between a first advanced position in which the sample notch of the toothed rack projects from the distal end portion of the cutting cannula, and a second retracted position in which the sample notch is in a proximal position with respect to the distal end portion of the cutting cannula in which the at least one tissue sample can be transferred from said sample notch. The cutting cannula and/or the toothed rack with the

sample notch are preferably independently movable in response to directions from a user of the biopsy device. A transport mechanism, e.g. in the form of an actuator system, may be provided to move the toothed rack. The transport mechanism may comprise a toothed wheel configured for engagement with the toothed rack.

**[0009]** The inner member may form a hollow needle wherein the biopsy device is configured to longitudinally displace a severed tissue sample inside the hollow needle in a proximal direction from the sample notch to a collection position where the tissue sample can be collected, e.g. transferred into a tissue collection tank. The longitudinal displacement may be provided by means of a vacuum delivered through the hollow needle.

**[0010]** The biopsy device is preferably adapted for being handheld by the user during harvesting of a tissue sample.

**[0011]** The present disclosure also relates to a disposable unit for a biopsy device for harvesting at least one tissue sample from a suspect tissue mass in a body of a living being comprising a cutting cannula that is hollow, an inner member comprising a sharpened distal tip configured to be introduced into the body and a sample notch for receiving the at least one severed tissue sample, the inner member receivable in the cutting cannula, and a cutting mechanism configured for causing the cutting cannula to be longitudinally displaced in a distal direction from a first position at the proximal end of the sample notch exposing the sample notch, to a second position at the distal end of the sample notch, so as to sever said tissue sample from remaining body tissue at the harvesting site. The disposable unit may further comprise an interface for connecting the disposable unit to a handle unit.

#### BRIEF DESCRIPTION OF THE DRAWINGS

**[0012]** The invention will be described in further detail with reference to the drawings in which:

Fig. 1 is an exemplary embodiment of a biopsy device according to the invention.

Fig. 2 is an exploded view of the components in Fig. 1.

Fig. 3 is a detailed view of a rigid toothed rack with a sharpened tip and sample notch at the distal end and a rotation zone in the proximal end.

Fig. 4a shows a cutting cannula in an advanced position covering a sample notch.

Fig. 4b shows a cutting cannula in a retracted position exposing a sample notch.

Fig. 5 shows a damper spring for use in connection with overshoot of a spring-loaded cutting cannula.

Fig. 6 shows a counter-rotation cutting interface between a sample notch and a cutting cannula.

Fig. 7 is a cross-sectional view of a cutting cannula featuring a longitudinal air channel having a lateral vent hole.

Fig. 8a shows a tissue collection tank.

Fig. 8b is a cut through illustration of the tissue collection tank in Fig. 8a.

Fig. 9 illustrates the cutting interface between a cutting cannula and a protrusion at the inner member forming a cutting board for the cutting cannula. A cut-out in the drawing shows the longitudinal air channel and a plurality of vent holes in the cutting cannula.

**[0013]** Corresponding reference characters indicate corresponding parts throughout the several views. The exemplifications set out herein illustrate embodiments of the invention and such exemplifications are not to be construed as limiting the scope of the invention in any manner.

#### DETAILED DESCRIPTION OF THE INVENTION

**[0014]** The drawings illustrate exemplary biopsy devices which are provided with a needle portion comprising a cutting cannula 1,1' and a sample notch 3 with a sharpened distal tip 4 for piercing tissue. The cutting cannula 1 is provided with a slanted cutting profiled as illustrated e.g. in Figs. 2 and 6, whereas the cutting cannula 1' is provided with a straight cutting profile 24 as illustrated e.g. in Figs. 5, 7 and 9. The sample notch 3 is part of a rigid toothed rack 2, and is movable between a first advanced and a second retracted position when actuated by a suitable source of mechanical motion. The source of mechanical motion may be a motor that may be powered by a battery and operatively connected to the rigid toothed rack 2 by means of one or more gear wheels 11.

**[0015]** The operative connection between the rigid toothed rack 2 and the gear wheels 11 is configured to permit full 360 degree rotation of the toothed rack 2, including the sample notch 3, about its longitudinal axis. Such rotation may for instance be permitted by providing a proximal rotation zone 12 with a series of cut-outs that run around the entire circumference of the toothed rack. A rotation control gear 9, that is in operative connection with the rigid toothed rack, is engaged by a rotation driver gear 10 to support the rotation of the rigid toothed rack 2 about its longitudinal axis. Another set of gearwheels may be in operative engagement with the cutting cannula 1 to provide full 360-degree rotation of the cutting cannula 1 either independently or in step with the rotation of the rigid toothed rack 2.

**[0016]** The cutting cannula 1,1' may be retracted when actuated by a suitable source of mechanical motion. In the first embodiment, the source of mechanical motion may be a second motor that is powered by a battery and operatively connected to the cutting cannula 1, 1' by means of a series of gears driving an actuator rod. Retraction of the cutting cannula 1, 1'

exposes the sample notch 3, 3', and permits tissue to prolapse into the lateral opening of the sample notch 3, 3'.

**[0017]** During or after retraction of the cutting cannula 1, 1', a vacuum may be switched on to support the prolapsing of tissue into the sample notch 3, 3'. Vacuum is communicated from a vacuum pump and a hose through a vacuum gasket 7 that is in operative connection with the cutting cannula 1, 1' and into the inner lumen of cutting cannula 1, 1'. The rigid toothed rack 2 is provided with at least one vacuum cut-out 16 that run along the length of the rigid toothed rack 2, and end in sample notch 3, and the vacuum from the vacuum pump is communicated through these vacuum cut-outs 16 to the sample notch 3 as soon as the pump is turned on.

**[0018]** A vacuum accumulator/reservoir may be configured to build and store a vacuum, is also in fluid communication with the sample notch 3, 3', and may provide a transient boost to the vacuum strength immediately prior to firing of the cutting cannula 1, 1' to increase sample size.

**[0019]** Retraction of the cutting cannula 1, 1' cocks a spring-loaded firing mechanism that is capable of powering the cutting cannula forward (i.e. in a distal direction) at high speed. As the cutting cannula 1, 1' moves forward at high speed, the sharpened distal end of the cannula 1, 1' makes contact with the tissue that has prolapsed into the sample notch 3, 3' and severs it from the surrounding connecting tissue.

**[0020]** As illustrated in Fig. 5 the cutting cannula 1' may be permitted to continue its travel by a damper spring 13 that is placed in a damper spring housing 14 and is in operative connection with a rear flange 15 of the cutting cannula 1'. The inertia of the cutting cannula 1' will allow it to proceed 1-2 mm beyond the permissible traveling distance of the spring-loaded firing mechanism, and will ensure that the sharpened distal end of the cutting cannula 1' has achieved a suitable overlap with the distal section of the sample notch 3'. Following the overthrow, the damper spring 13 ensures that the cutting cannula 1' is returned to its neutral position in preparation for the next tissue sample.

**[0021]** As illustrated in Fig. 6 the user of the biopsy device has the option of rotating the toothed rack 2 with the sample notch 3 relative to the stationary cutting cannula 1 to sever any connective tissue that has not been completely severed by the cutting cannula 1. Connective tissue that has not been completely severed may restrict retraction of the tissue sample and cause pain to the patient. The rotation causes connective tissue that has not been completely severed to saw against the sharpened distal end of cutting cannula 1 for as long as needed to complete the severing. Rotation may be step-wise and may interchange between a clockwise and a counter-clockwise direction and take place over a rotation angle of e.g. +/- 20 degrees relative to a neutral position. Furthermore the cutting cannula 1 may be retracted and advanced in steps of 1-2 mm during rotation to further support the severing of tissue. When unrestricted movement of the sample notch 3 has been restored, the toothed rack 2 may continue its motion from the first advanced to the second retracted position to transport the tissue sample in sample notch 3 out of the body of the patient.

**[0022]** The tissue sample may be collected in a tissue collection tank 8 comprising a vacuum spout 21 through which a vacuum from a vacuum pump or vacuum accumulator may be communicated into a collection tank chamber 22. From the collection tank chamber, the vacuum may be communicated through a tissue collection spout 23 for enhanced collection of the tissue sample. As illustrated in Fig. 8b the collection spout 23 forms a collection tube 23' inside the collection tank 22 extending with a certain length from the bottom of the tank 22. Following collection of the tissue sample from the sample notch 3, said sample notch 3 may be returned to the sampling site for collection of the next tissue sample.

**[0023]** As illustrated in Figs. 7 and 9 the cutting cannula may have an inner tube 17 and an outer tube 18 forming between them a longitudinal air channel 19 that is at a proximal end in fluid communication with a first vacuum pump through a two-way valve that may be switched between a vacuum position and a position that permits entry of atmospheric air into the air channel. At the distal end the air channel 19 is in fluid communication with the lateral opening of the sample notch 3 through at least one vent hole 20 that is formed in the inner tube 17.

**[0024]** As illustrated in Fig. 9 a plurality of the vent holes 20 may be distributed circumferentially around the inside of the inner tube 17. As illustrated in Fig. 9 a protrusion 25 formed as a collar may be provided adjacent to the sharpened distal end 4'. The interface 26 between the protrusion 25 and the cutting cannula 1' forms a cutting board to ensure that connective tissue is cut properly during severing.

**[0025]** A frequently encountered complication in the harvesting of tissue samples is the presence of fibrous or connective tissue. Such tissue is characterized by being highly resilient and difficult to cut. The typical manifestation of malfunctions related to connective tissue is that the biopsy device gets stuck in the body of the patient and has to be removed by force or surgical intervention. This may be stressful to both physician and patient and may additionally be very painful for the patient. Inadequately severed connective tissue is a known problem for all kinds of biopsy devices and the problem is highly undesirable.

**[0026]** The use of a linear cutter requires a very precise interplay between the sharpened distal end of the cutting cannula and the distal section of the sample notch if appropriate severing of connective tissue is to occur. For this reason it is important that the position of the sample notch is very precisely controlled relative to the position of the cutting cannula. SIMS devices featuring a linear, spring-loaded cutting cannula typically employ a sample notch that is attached to a flexible bendable elongate member (e.g. a non-rigid toothed rack), and this toothed rack may not always produce the desired control of position of the sample notch due to the flexibility, design and material chosen. Some prior art devices employ toothed racks made of thermoplastic elastomers with significant longitudinal elasticity. By having the sample notch in a rigid toothed rack, which is longitudinally inelastic, a better control of position is provided. Thereby an appropriate overlap of the sharpened end of the cutting cannula with the distal section of the sample notch can be provided. Failure to establish a precise position of the sample notch may result in the incomplete closing of the sample notch opening. A rigid toothed rack provides the necessary lateral inelasticity and stability to ensure that the sharpened distal

end of the cutting cannula completely closes the opening of the sample notch. Employing a rigid toothed rack therefore provides an improved control of the longitudinal and lateral position of the distal sharpened end of the cutting cannula relative to the distal section of a sample notch.

**[0027]** In one embodiment the proximal end of the rigid toothed rack is configured to operatively connect with a retraction gear wheel, and is furthermore configured to permit 360 degree rotation of the toothed rack about its longitudinal axis without requiring that the operative connection with the retraction gearwheel is interrupted. This may be provided by means of a rotation mechanism.

**[0028]** In a further embodiment of the invention the rigid toothed rack comprises a rotation zone in the proximal end with circumferential teeth, e.g. in the form of a series of cut-outs that run around the entire circumference of the toothed rack, thereby permitting rotation of the rigid toothed rack. The rigid toothed rack may be rotatable within the cutting cannula and/or the rigid toothed rack and the cutting cannula are rotatable simultaneously relative to the biopsy device. The permitted rotation may be 360 degrees. The biopsy device may further comprise a rotation control gear attached to the rigid toothed rack. A rotation driver gear may be provided and configured to engage with the rotation control gear for rotation of the rigid toothed rack. The cutting cannula may also be configured to rotate, such as 360 degrees, about its longitudinal axis.

**[0029]** In a further embodiment of the invention the rigid toothed rack is configured such that longitudinal displacement of the rigid toothed rack to the second retracted position can only be provided in a predefined rotational orientation of the rigid toothed rack. Thus, the rigid toothed rack may be rotatable within the cutting cannula only in the first advanced position, and/or the rigid toothed rack and the cutting cannula are rotatable simultaneously relative to the biopsy device only in the first advanced position.

**[0030]** Whether the rigid toothed rack and/or the cutting cannula is rotated simultaneously or independently may at least partly be controlled by means of an interlock mechanism configured for fixing the rigid toothed rack and the cutting cannula relative to each other. E.g. the interlock mechanism may have two states, one state that allows free movement of the cutting cannula and the toothed rack relative to each other and one state that fixes the two to each other.

**[0031]** This may help to ensure that the sample notch is always oriented correctly with respect to a tissue collection tank when a tissue sample is transferred to the tank. This may be provided if the toothing of the toothed rack is only located at one side of the rigid toothed rack. If there is a proximal rotation zone of the toothed rack as mentioned above, the toothing that extends in the distal direction beyond the rotation zone is only located at one side of said rigid toothed rack. A control system may help to ensure that the rigid toothed rack has the correct rotational orientation before retracting to the retracted position.

**[0032]** Rotation of the rigid toothed rack relative to the cutting cannula (or vice versa) may be advantageous during severing of a tissue sample and may thereby be an improvement of the cutting mechanism. Rotation of the toothed rack, and thereby the sample notch, relative to the cutting cannula with the sharpened distal end, may result in a "sawing" motion that may complete the severing of incompletely severed connective tissue. Counter-rotation of the cutting cannula and the rigid toothed rack may further be provided during cutting which allows for enhanced cutting of e.g. connective tissue.

**[0033]** Thus, in one embodiment of the invention the rigid toothed rack is rotatable within the cutting cannula during severing of the at least one tissue sample. The cutting mechanism may be configured to rotate the rigid toothed rack within the cutting cannula during severing of the at least one tissue sample. The rotation may be either stepwise or continuous. The rigid toothed rack and/or the cutting cannula may be rotatable in clockwise and/or in counter-clockwise directions. During severing the rotation angle of the rigid toothed rack relative to the cutting cannula may oscillate between -5 and +5 degrees during severing, more preferably between -10 and +10 degrees, more preferably between - 15 and +15 degrees, more preferably between -20 and +20 degrees, more preferably between -25 and +25 degrees, more preferably between -30 and +30 degrees, i.e. like a sawing motion oscillating between clock-wise and counter clock-wise directions.

**[0034]** When taking a biopsy it is often necessary to rotate the entire biopsy device inside the patient in order to position the sample notch against the suspect tissue mass. This may lead to awkward handling situations during harvesting of tissue samples. A further advantage of rotational capability is therefore that the rigid toothed rack and the cutting cannula can be rotated simultaneously, preferably controlled by the user, about their longitudinal axis relative to the biopsy device in order to orientate the sample notch towards the suspect tissue mass, e.g. prior to activation of the firing mechanism. Thus, the biopsy device can be held in a steady position while the rigid toothed rack and the cutting cannula are rotated into the correct angular orientation relative to the suspect tissue mass.

**[0035]** Another way to enhance the correct severing of tissue is if the cutting mechanism is configured to interchangeably retract and advance the cutting cannula in small longitudinal steps during severing of a tissue sample. The size of the steps may be between 0 and 3 mm, or between 0 and 1 mm, or between 1 and 2 mm or between 2 and 3 mm. This corresponds to a sawing motion in the longitudinal direction.

**[0036]** The cutting mechanism may also be improved if it is configured to provide a predefined overlap and/or overshoot during severing of a tissue sample such that the distal end of the cutting cannula passes beyond the distal end of the sample notch temporarily before returning to said second position. The length of said overshoot may be between 0.5 and 5 mm, or between 0.5 and 1 mm, or between 1 and 2 mm, or between 2 and 3 mm, or between 3 and 4 mm, or between 4 and 5 mm. This overshoot of the cutting cannula may help to apply further stress to incompletely severed tissue. The overshoot may be provided by means of an elastic element provided in connection with the cutting cannula. One solution could be in the form of at

least one damper spring mounted in a damper spring housing. The damping may also be provided by using a damping element formed in rubber. The elastic element may be configured to work along with a firing mechanism of the cutting cannula effected during severing of a tissue sample. If the firing mechanism is stopped by the elastic element the inertia of the cutting cannula and the elasticity of the elastic element will allow the sharpened end of the cutting cannula to proceed a certain length beyond the traveling distance of the spring-loaded firing mechanism, and thereby ensure that the sharpened distal end of the cutting cannula achieves a suitable overlap with the distal section of the sample notch. Subsequent to this overshoot, the elastic element ensures that the cutting cannula can be returned to its neutral position in preparation for the next tissue sample.

**[0037]** As an alternative, or supplement to, an overlap or overshoot between the distal sharpened end of the cutting cannula and the distal section of the sample notch, the inner member may further comprise a circumferential protrusion and/or collar located between the sharpened distal end and the sample notch, said circumferential protrusion formed to match the distal end of the cutting cannula. The circumferential protrusion may thus be configured to form a cutting surface for the cutting cannula during severing of a tissue sample. The cutting board (protrusion) may be disposed about the outer periphery of the sample notch and serve the purpose of ensuring that the tissue sample is completely and cleanly severed by the cutting cannula. The cutting mechanism may be configured such that the cutting cannula and the circumferential protrusion encounter during severing of a tissue sample. The protrusion is then preferentially formed in a material that is softer than the cutting cannula in order not to blunt the cutting cannula and preserve the sharpness of the cutting cannula. The cutting mechanism may alternatively be configured such that the cutting cannula and the circumferential protrusion does not encounter during severing of a tissue sample. Thus, the circumferential protrusion may be brought into close proximity without encountering during severing of a tissue sample. I.e. direct physical contact between the protrusion and the sharpened distal end of the cutting cannula is avoided but established at the material surface in close proximity to said sharpened distal end. With such a protrusion the transport of the tissue sample must be provided through the inside of the inner member, typically by means of vacuum, if SIMS functionality is desired.

**[0038]** In a further embodiment of the invention the cutting cannula comprises at least one longitudinal vacuum channel (aka longitudinal air channel or passage) formed inside the external shell / wall of the cutting cannula. The longitudinal vacuum channel may be circumferential. This air channel may be provided by forming the cutting cannula as an inner and an outer tube forming between them an air passage that runs longitudinally along the length of the inner and outer tube. Fluid communication from this air channel and into the inner lumen of the cutting cannula may be provided by one or more lateral vent holes extending from the inside of the cutting cannula to the longitudinal air channel. A plurality of said lateral vent holes may be distributed circumferentially in the cutting cannula. The longitudinal vacuum channel may then, in its distal end, be in fluid communication with the sample notch when the rigid toothed rack is in its first advanced position. Thereby the cutting cannula may be configured such that a vacuum or air flow can be provided and/or established inside the cutting cannula, e.g. an airflow from the air channel and into the inner lumen of the cutting cannula.

Fluid communication from this air channel and to the external of the cutting cannula may be provided by at least one vacuum spout and may be controlled by at least one vacuum valve. A vacuum pump may then be connected to the air channel via this vacuum valve, in which case a vacuum may be communicated through the air channel and the air vent holes and into the inner lumen of the cutting cannula. Thus, air may be sucked out of the inner lumen of the cutting cannula. Such evacuation may be useful for reducing or eliminating problems with air that has been accidentally introduced in the biopsy cavity and disturbs image quality in an ultrasound-guided biopsy procedure. Unwanted air may be introduced in the biopsy cavity when the rigid toothed rack is being advanced from the second retracted position and to the first advanced position. This advancement of the rigid toothed rack inside the cutting cannula may function as a piston that compresses the air inside the cutting cannula and this air is consequently blown into the biopsy cavity disturbing the ultrasound picture. If air is evacuated from the cutting cannula through the longitudinal vacuum channel inside the sidewall of the cutting cannula during advancement of the rigid toothed rack this problem can be addressed and solved.

**[0039]** A further embodiment of the invention comprises a tissue collection tank for collecting the at least one tissue sample transferred from the sample notch. The tank may comprise a tissue-collecting spout that may be configured to slide into the sample notch chamber and scoop the tissue sample into a sample tank. To enhance the collection of the tissue sample the tissue collection tank may be configured to be vacuumized, e.g. by connection to a vacuum pump via a vacuum port at the tank. The collecting spout may be elongated to form a pipe (aka collection pipe) to enhance the vacuum assisted collection of a tissue sample into the tank. At the outside the collection spout / pipe forms a small spout but at the inside of the tissue collection tank the collection pipe extends and/or protrudes into the tissue collection tank, i.e. the collection pipe may protrude from the bottom or side of the inside of the tissue collection tank. Thus, the collection pipe has a certain length inside the tissue collection tank. This length of the collection pipe may be at least 2 mm, or at least 4 mm, or at least 6 mm, or at least 8 mm, or at least 10 mm, or at least 12 mm, or at least 14 mm, or at least 16 mm, or at least 18 mm, or at least 20 mm, or at least 22 mm, or at least 24 mm, or at least 26 mm, or at least 28 mm, or at least 30 mm, or at least 32 mm, or at least 34 mm, or at least 36 mm, or at least 38 mm, or at least 40 mm.

**[0040]** Some biopsy devices are constantly connected to external vacuum pumps via external vacuum hoses. These pumps can deliver a powerful and constant vacuum to the biopsy device but the necessary vacuum hoses reduce the manageability of the biopsy device for the user. A solution to that problem has until now been to provide one or more local battery driven small vacuum pumps integrated in the biopsy device. However, such small vacuum pumps can only provide a limited airflow which sometimes is not sufficient to maintain a constant vacuum level. A solution to that problem can be a vacuum reservoir integrated in the biopsy device that can deliver a boost to the (negative) airflow for one or more short periods of time, this additional airflow provided by the vacuum reservoir can thereby maintain a certain vacuum level. The biopsy device can thereby be provided with one or more small vacuum pumps supplied by the vacuum reservoir when necessary. A further embodiment therefore comprises a vacuum

reservoir (aka vacuum accumulator) configured for accumulating a volume of vacuum that can be delivered as a transient boost in the airflow so as to maintain a level of vacuum present in the system. Such a vacuum reservoir can for instance be powered by a battery. The vacuum reservoir may be in fluid communication with the sample notch and configured to provide an increased suction to maintain the vacuum level in the sample notch during severing of a tissue sample, e.g. immediately before release of the cutting cannula in order to increase the amount of tissue that prolapses into the sample chamber and thereby maximize the size of the severed tissue sample. The vacuum reservoir may also be in fluid communication with the inside of the hollow inner member and configured to provide a transient boost of airflow when a tissue sample is being sucked through the inner member. Furthermore, the vacuum reservoir may be in fluid communication with the tissue collection tank and configured to provide a vacuum to or an increased suction in the tissue collection tank to main a vacuum level when a tissue sample is transferred from the sample notch and into the tissue collection tank. The vacuum reservoir may have a volume of 5-100 mL, or 5-10 mL, or 10-20 mL, or 20-30 mL, or 30-40 mL, or 50-100 mL.

**[0041]** Retraction of the cutting cannula to expose the sample notch may for instance be actuated by a motor that is powered by a battery and connected to one or more gearwheels, but other power sources and means of mechanical actuation are also envisioned. This retraction of the cutting cannula may facilitate the cocking of a firing mechanism that may for instance be spring-loaded. Other firing mechanisms, including electric, pneumatic and chemical, may also be provided. The cutting movement of the cutting cannula during the actual severing of tissue may be powered by the energy that is stored in a firing mechanism and happens as a high-speed linear passage across the laterally facing opening of the sample notch. During this passage, the sharpened distal end of the cutting cannula makes contact with the tissue that has prolapsed into the sample notch chamber and severs it from the surrounding tissue, thus creating a tissue sample in the sample notch. The firing mechanism may be replaced with a linear actuator that allows the controlled advancement of the cutting cannula during severing. In this case advancement of the cutting cannula is more controlled and it may be desirable to rotate the cutting cannula during advancement to adequately sever the tissue as described previously.

**[0042]** To provide for SIMS functionality retraction of the sample notch may be provided by means of a motor that is operatively connected to the rigid toothed rack by means of one or more gearwheels. When activated, this motor causes the rigid toothed rack and the sample notch to travel from the first advanced position to the second retracted position, where the sample may be retrieved, e.g. by means of a tissue collection tank, but other means of retrieval - including manual retrieval - may also be envisioned. After completion of sample retrieval, the sample notch may be returned to the sampling site by reversing the direction of rotation of the motor.

**[0043]** The firing mechanism may be configured for causing the cutting cannula and the inner member to be longitudinally displaced in a distal direction, so as to penetrate body tissue at or near the suspect tissue mass prior to the cutting operation when harvesting a sample.

**[0044]** In one embodiment the inner member comprises a vacuum port in fluid communication with the sample notch. The inner member may thus be configured such that the sample notch can be vacuumized. A vacuum pump may be provided for generating a suction effect in the sample notch to increase the size of the tissue sample that prolapses into the sample notch, the vacuum pump being in fluid communication with the sample notch through a longitudinally extending passage in the inner member.

**[0045]** A further embodiment comprises a handle unit with a power source and at least one motor for driving the cutting mechanism and the displacement of the inner member and wherein at least the cutting cannula and the inner member are comprised in a disposable unit, which is releasably secured to the handle unit.

**[0046]** To ensure that the cutting cannula and the sample notch achieve an overlap that is sufficient to cleanly sever the tissue to be sampled, the cutting cannula is preferably characterized by very tight length tolerances. Such tolerances may be achieved by the use of materials with low creep that are processed using high-precision milling or molding, and possibly result in total length variations of no more than +/- 0.5 mm depending on the overall total length of the cutting cannula. A preferred material for the cutting cannula is stainless steel which is made into tubes. These tubes are typically made by rolling and welding sheet metal to form a tubular structure which is then drawn through a tool with a diamond insert to achieve the desired diameter. Multiple drawings may be employed to achieve high precision. By utilizing stainless steel low creep for the cutting cannula, none or minimal elongation and achievable manufacturing tolerances are possible. Other materials, including titanium, are also envisioned for the making of the cutting cannula.

**[0047]** To further support appropriate overlap between cutting cannula and sample notch, also the rigid toothed rack may be characterized by very tight length tolerances. Such tolerances may in some embodiments be achieved by the use of materials with low creep that are processed using high-precision milling or molding, and possibly result in total length variations of no more than +/- 0.5 mm depending on the overall total length of the rigid toothed rack. A preferred material for the rigid toothed rack is stainless steel. The rigid toothed rack would typically be made by milling a turned stainless steel metal rod in order to achieve the desired geometry. Other materials suited for the rigid toothed rack are titanium or similar metals with a high modulus of elasticity. Alternative materials include thermoplastic elastomers with suitable fillers for increased modulus of elasticity. Suitable types for a rigid toothed rack would be LCP (Liquid Crystal Polymer), PEEK (Polyetheretherketone) in any grade. Thermoplastic elastomers have the benefit of being relatively easy to process and manufacture, but they are less rigid and will also tend to creep and shrink more than metal.

**[0048]** This application is therefore intended to cover any variations, uses, or adaptations of the invention using its general principles. Further, this application is intended to cover such departures from the present disclosure as come within known or customary practice in the art to which this invention pertains and which fall within the limits of the appended claims.

## REFERENCES CITED IN THE DESCRIPTION

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### Patent documents cited in the description

- [WO2006005342A \[0004\]](#)
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- [WO2006005344A \[0004\]](#)
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- [EP0895752A1 \[0005\]](#)

**Patentkrav**

**1.** Engangsenhed til en biopsiindretning til at høste mindst én vævsprøve fra en suspekt vævsmasse i en krop af et levende væsen, omfattende:

en skærekanyle (1,1'), som er hul og har en distal ende;

5 et indre element, som inkluderer en stiv, roterbar tandstang (2), som har en tilspidset distal spids (4) konfigureret til at blive indført i kroppen og et prøveindsnit (3) til modtagelse af den mindst ene overskårne vævsprøve, hvor det indre element modtages i skærekanylen,

en skærmechanisme konfigureret til at forårsage skærekanylen at blive langsgående forskudt i en distal retning fra en første position ved den proksimale ende af prøveindsnittet som eksponerer prøveindsnittet, til en anden position ved den distale ende af prøveindsnittet, for således at afskære nævnte vævsprøve fra resterende kropsvæv ved høstningsstedet, at den stive, roterbare tandstang har en proksimal del og en rotationszone (12) i den proksimale del med periferisk fortanding der inkluderer en serie af udsnit der løber omkring hele omkredsen af den stive, roterbare tandstang for at tillade rotation af den stive, roterbare tandstang.

**2.** Engangsenheden ifølge krav 1, hvor det indre element er en hul nål.

20

**3.** Engangsenheden ifølge et hvilket som helst af kravene 1 og 2, hvor biopsiindretningen er konfigureret til langsgående at forskyde en overskåren vævsprøve inden i den hule nål i en proksimal retning fra prøveindsnittet til en samlingsposition, hvor vævsprøven kan overføres til en vævssamlingsbeholder 25 (22).

**4.** Engangsenheden ifølge krav 3, omfattende et vakuumreservoir i fluidforbindelse med prøveindsnittet og konfigureret til at tilvejebringe et øget sug og/eller opretholde vakuumniveauet i prøveindsnittet under afskæring af en 30 vævsprøve.

5. Engangsenheden ifølge et hvilket som helst af kravene 1 til 4, omfattende et rotationsstyringsgear (9) fastgjort til den stive, roterbare tandstang.

6. Engangsenheden ifølge et hvilket som helst af kravene 1 til 5, hvor det indre 5 element er langsgående forskydeligt i skærekanylen mellem en fremskreden position i hvilken prøveindsnittet af den stive, roterbare tandstang fremspringer fra skærekanylen og en tilbagetrukken position i hvilken prøveindsnittet er proksimal til den distale ende af skærekanylen.

10 7. Engangsenheden ifølge et hvilket som helst af kravene 1 til 5, omfattende en aflåsningsmekanisme konfigureret til at fiksere den stive, roterbare tandstang og skærekanylen i forhold til hinanden.

8. Engangsenheden ifølge et hvilket som helst af kravene 1 til 5, omfattende en 15 vævssamlingsbeholder (22), som har en vævssamlingstud (23), hvor biopsiindretningen er konfigureret til langsgående at forskyde en overskåren vævsprøve inden i den hule nål i en proksimal retning fra prøveindsnittet til en samlingsposition, hvor vævsprøven kan overføres til vævssamlingsbeholderen.

20 9. Engangsenheden ifølge krav 8, hvor vævssamlingsbeholderen har en vakuumport til tilvejebringelse af et vakuum inden i vævssamlingsbeholderen.

10. Engangsenheden ifølge et hvilket som helst af kravene 1 til 9, hvor den stive, 25 roterbare tandstang er roterbar inden i skærekanylen og/eller den stive, roterbare tandstang og skærekanylen er roterbare samtidig i forhold til biopsiindretningen, og/eller hvor rotationen af mindst én af den stive, roterbare tandstang og skærekanylen er trinvise.

30 11. Engangsenheden ifølge et hvilket som helst af kravene 1 til 10, hvor mindst én af den stive, roterbare tandstang og skærekanylen er roterbare i urets retning eller modsat urets retning.

**12.** Engangsenheden ifølge et hvilket som helst af kravene 1 til 10, hvor den stive, roterbare tandstang er konfigureret således at langsgående forskydning af den stive, roterbare tandstang til en tilbagetrukken position kun kan tilvejebringes i en foruddefineret rotationsorientering af den stive, roterbare tandstang.

5

**13.** Engangsenheden ifølge et hvilket som helst af kravene 1 til 12, hvor det indre element omfatter et periferisk fremspring (25) lokaliseret mellem den tilspidsede distale ende og prøveindsnittet, det periferiske fremspring er formet til at passe med den distale ende af skærekanylen, eventuelt hvor fremspringet er dannet i et 10 materiale, der er blødere end skærekanylen.

**14.** Engangsenheden ifølge et hvilket som helst af kravene 13, hvor det periferiske fremspring er konfigureret til at danne en skæreflade for skærekanylen.

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**15.** Engangsenheden ifølge et hvilket som helst af kravene 1 til 14, hvor skærekanylen har en udvendig skal og omfatter mindst en langsgående vakuumkanal dannet inden i den udvendige skal af skærekanylen, eventuelt hvor en distal ende af den langsgående vakuumkanal er i fluidforbindelse med det 20 indvendige af skærekanylen.

**16.** Engangsenheden ifølge et hvilket som helst af kravene 1 til 15, omfattende en flerhed af laterale udluftningshuller (20), som er fordelt periferisk i skærekanylen.

25

# DRAWINGS

Fig. 1

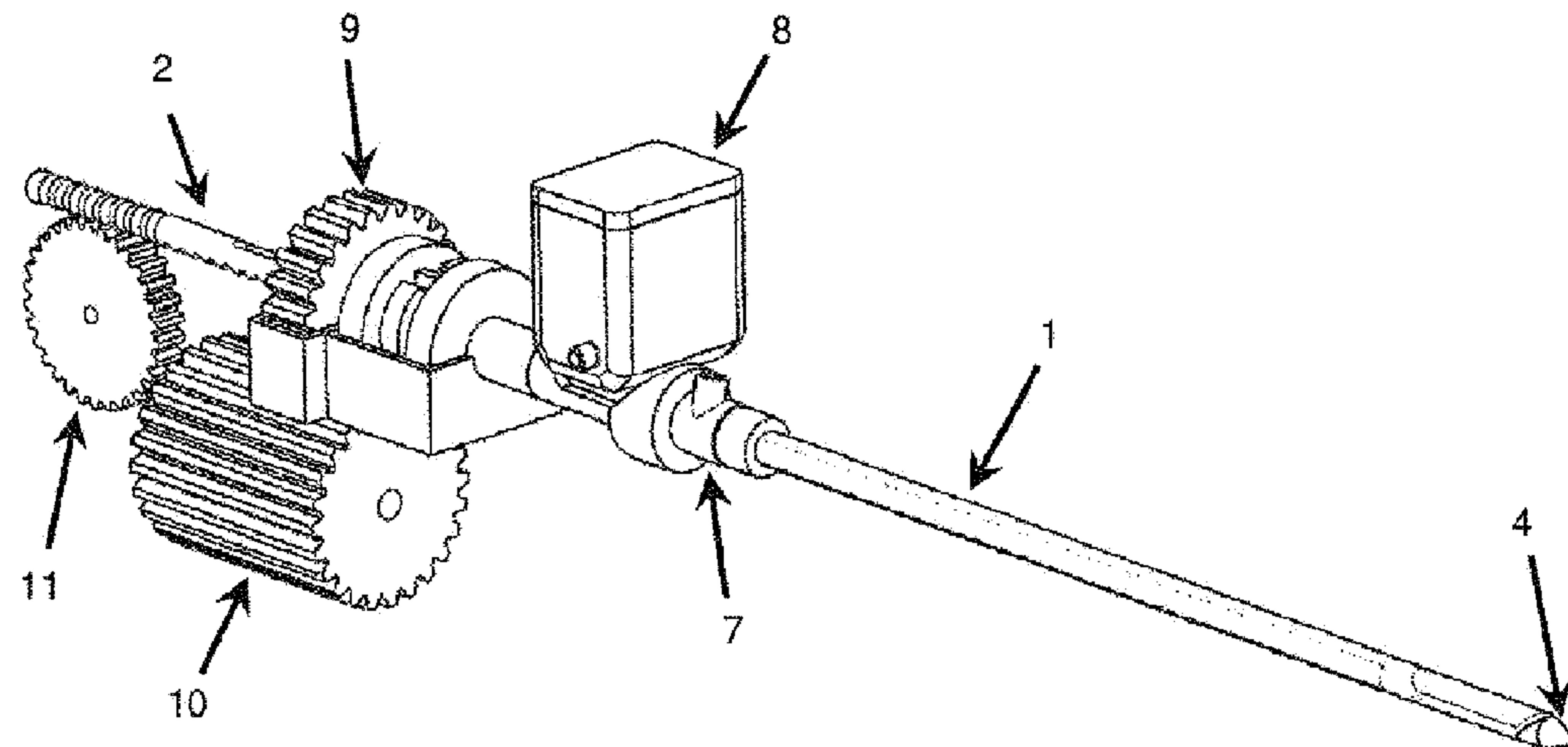


Fig. 2

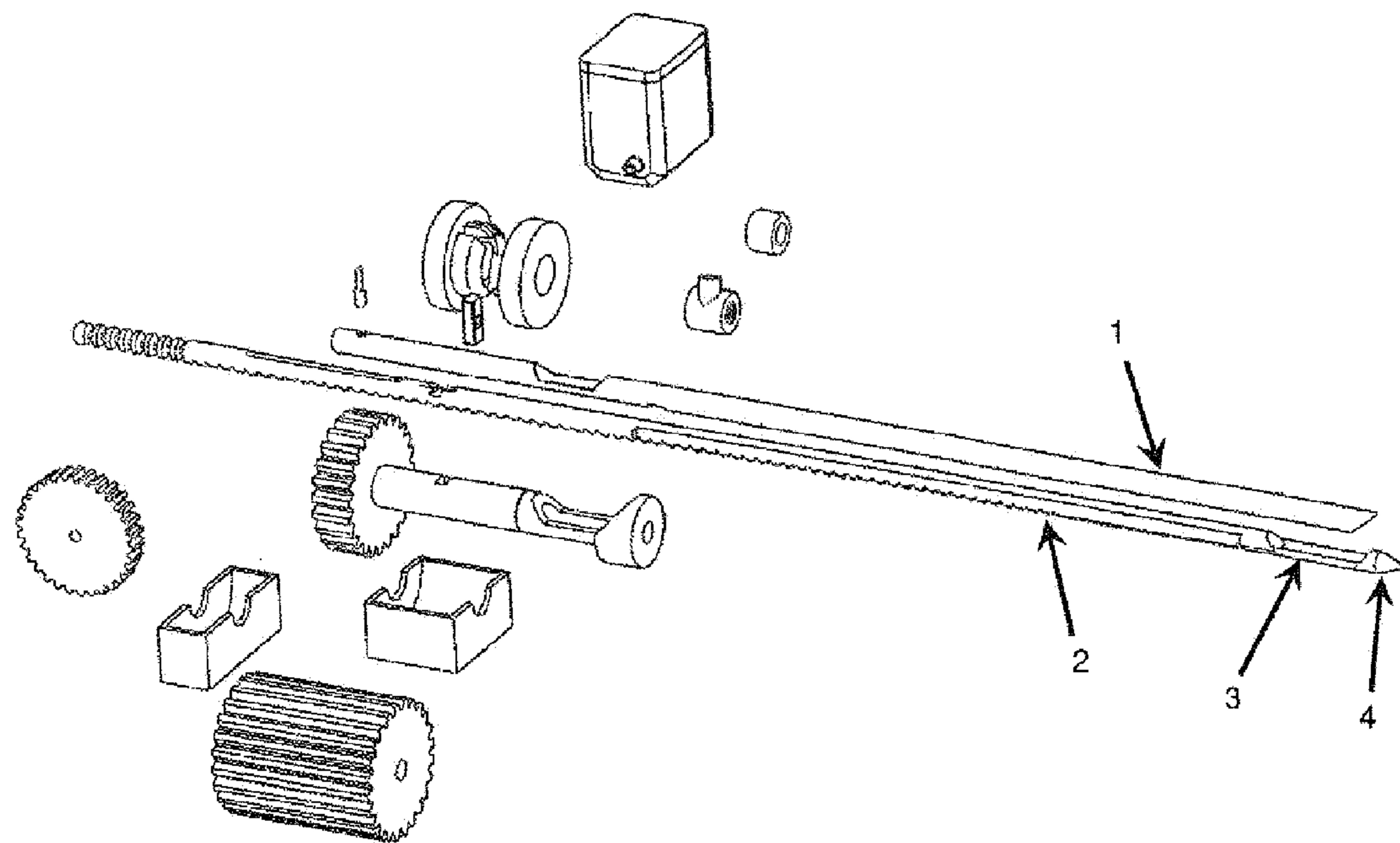


Fig. 3

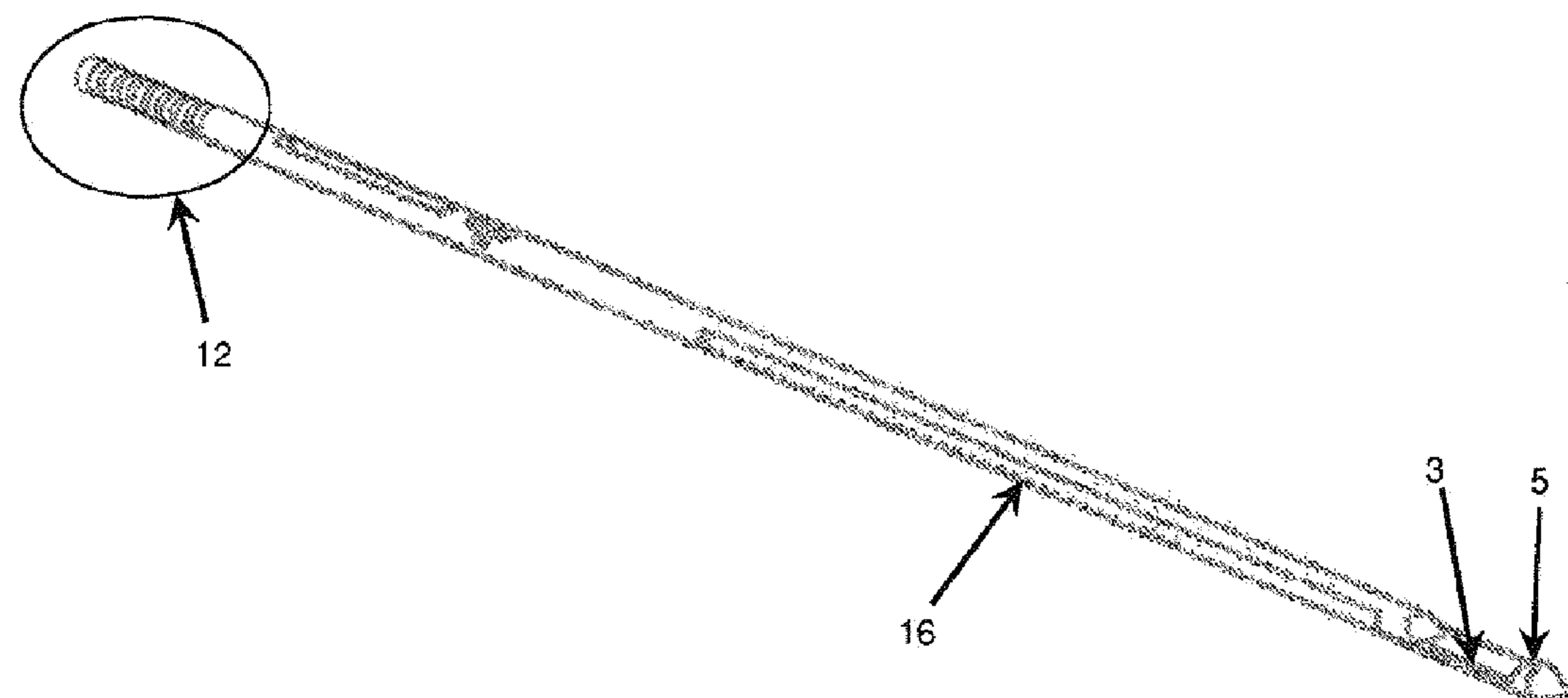


Fig. 4a

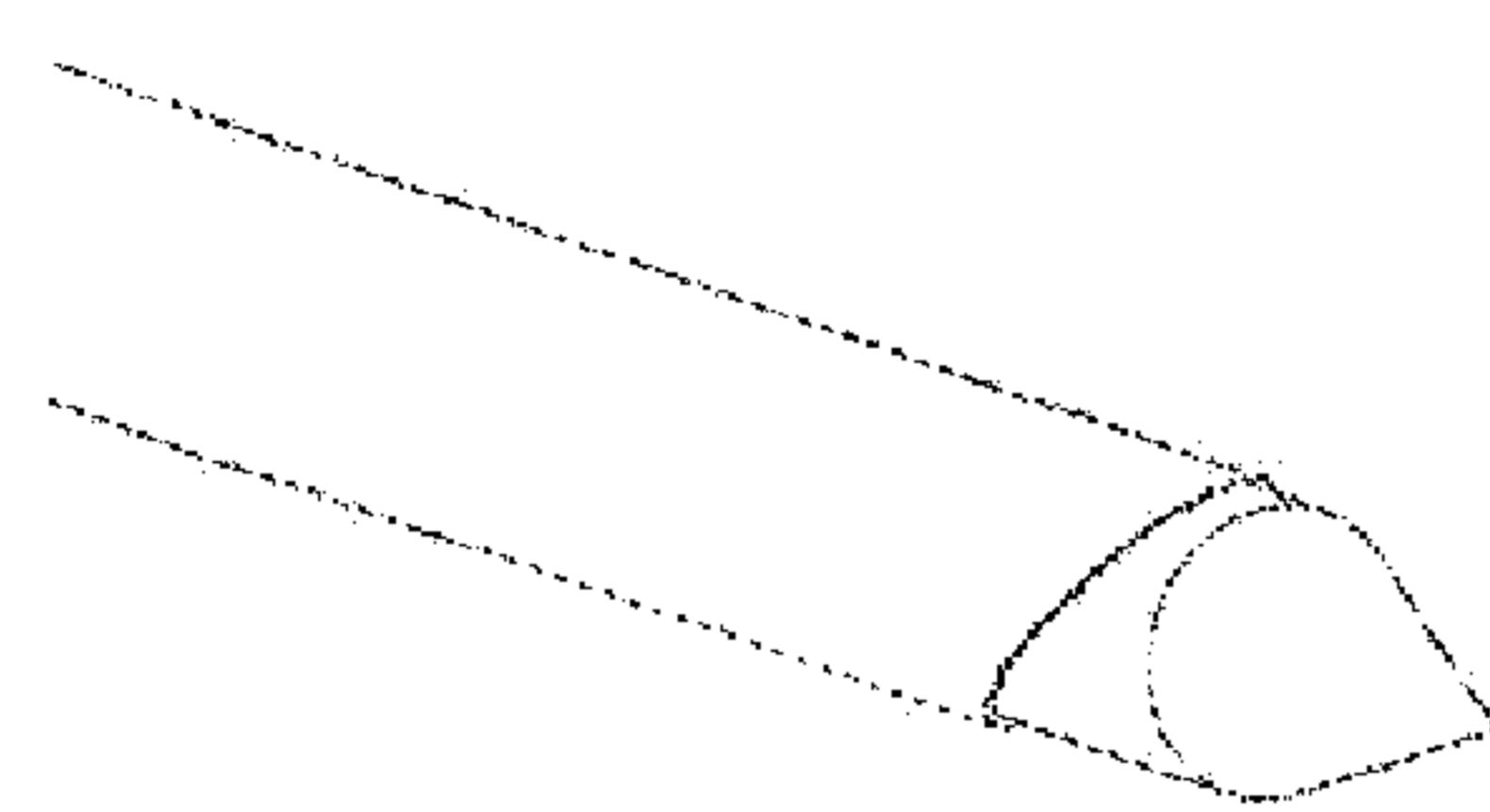


Fig. 4b

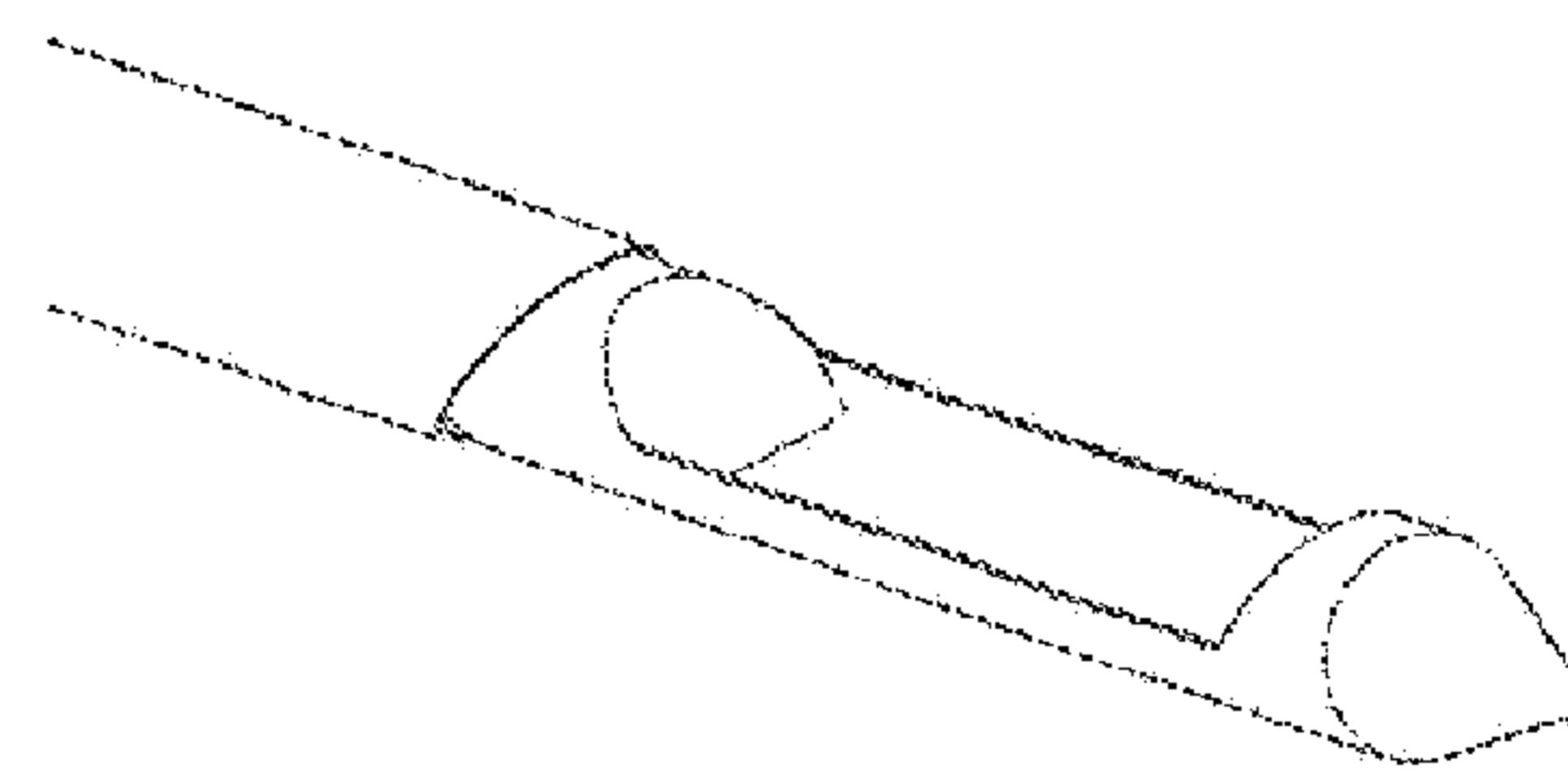


Fig. 5

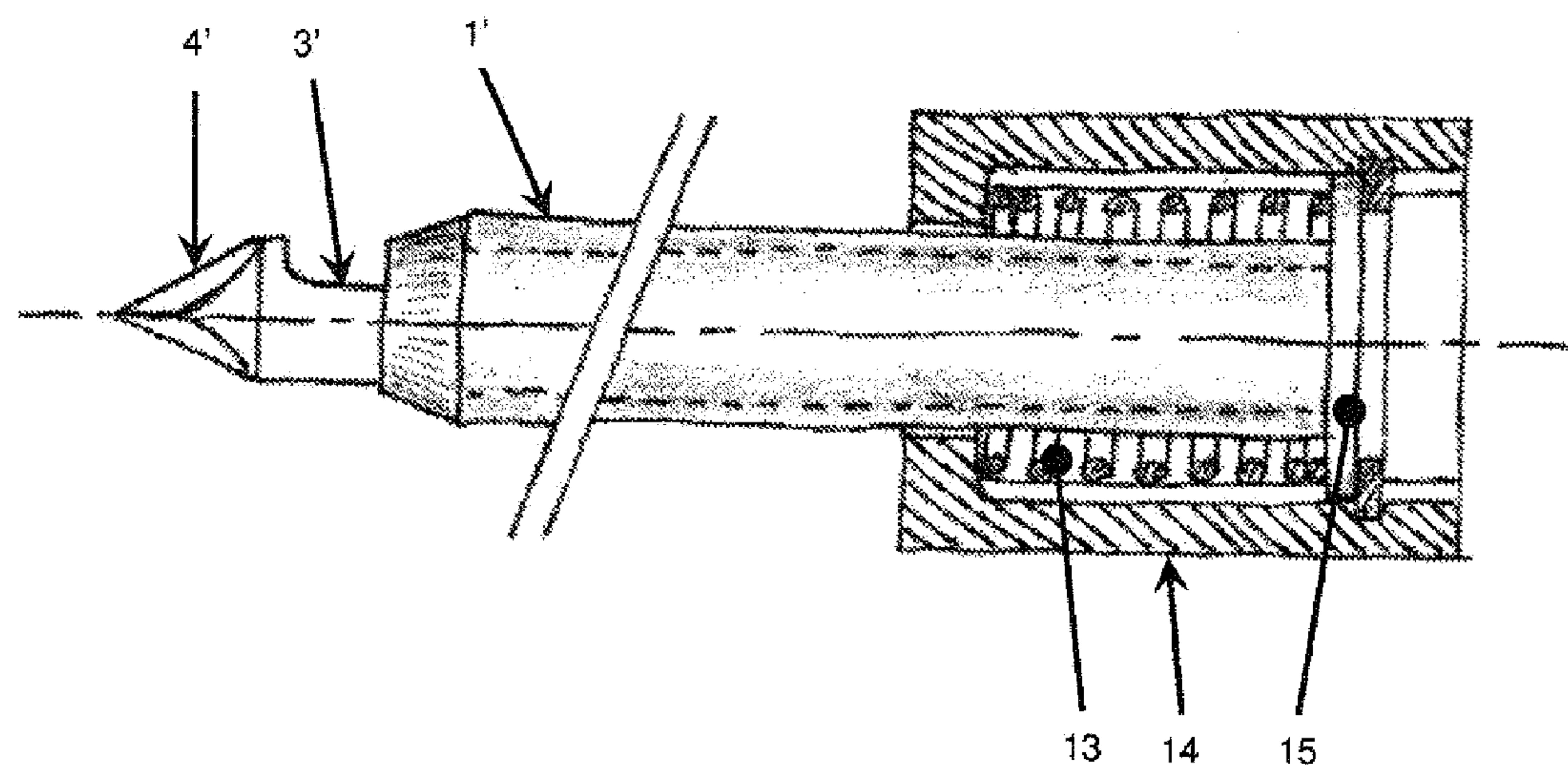


Fig. 6

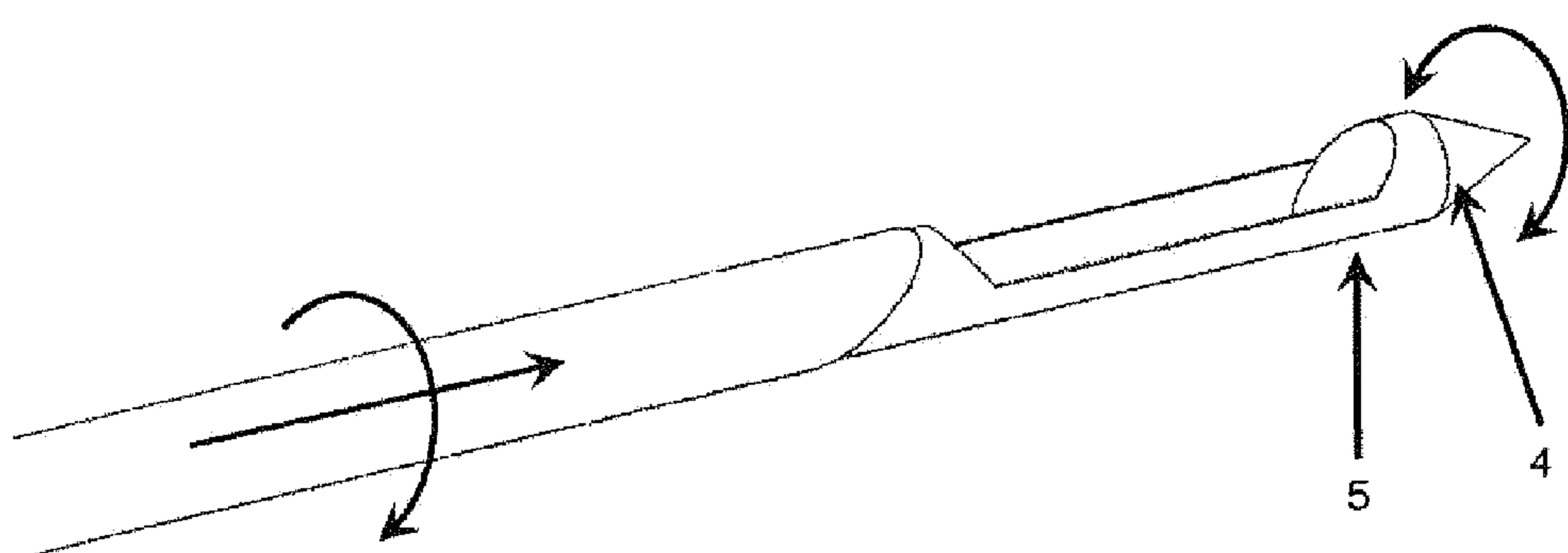


Fig. 7

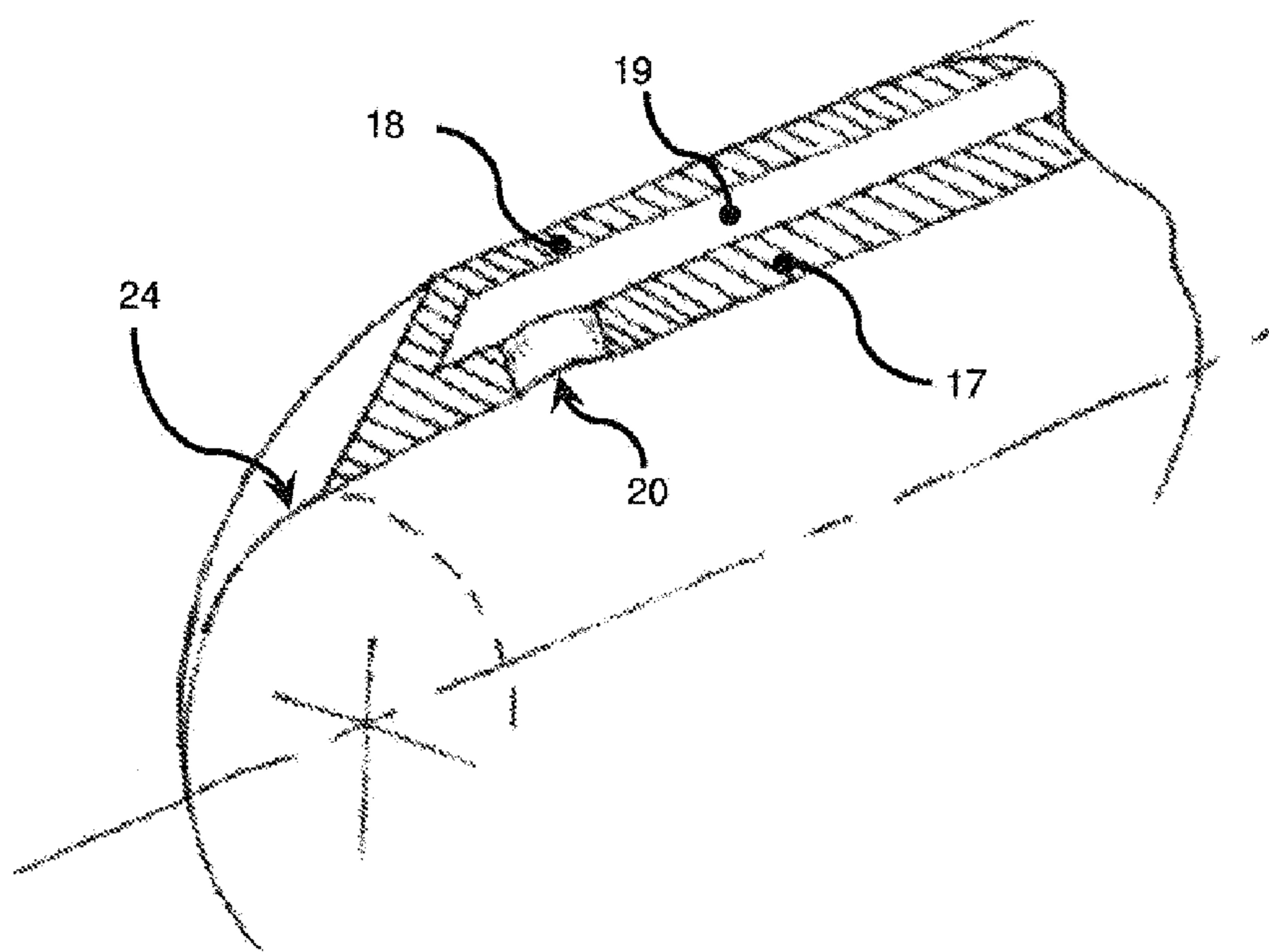


Fig. 8a

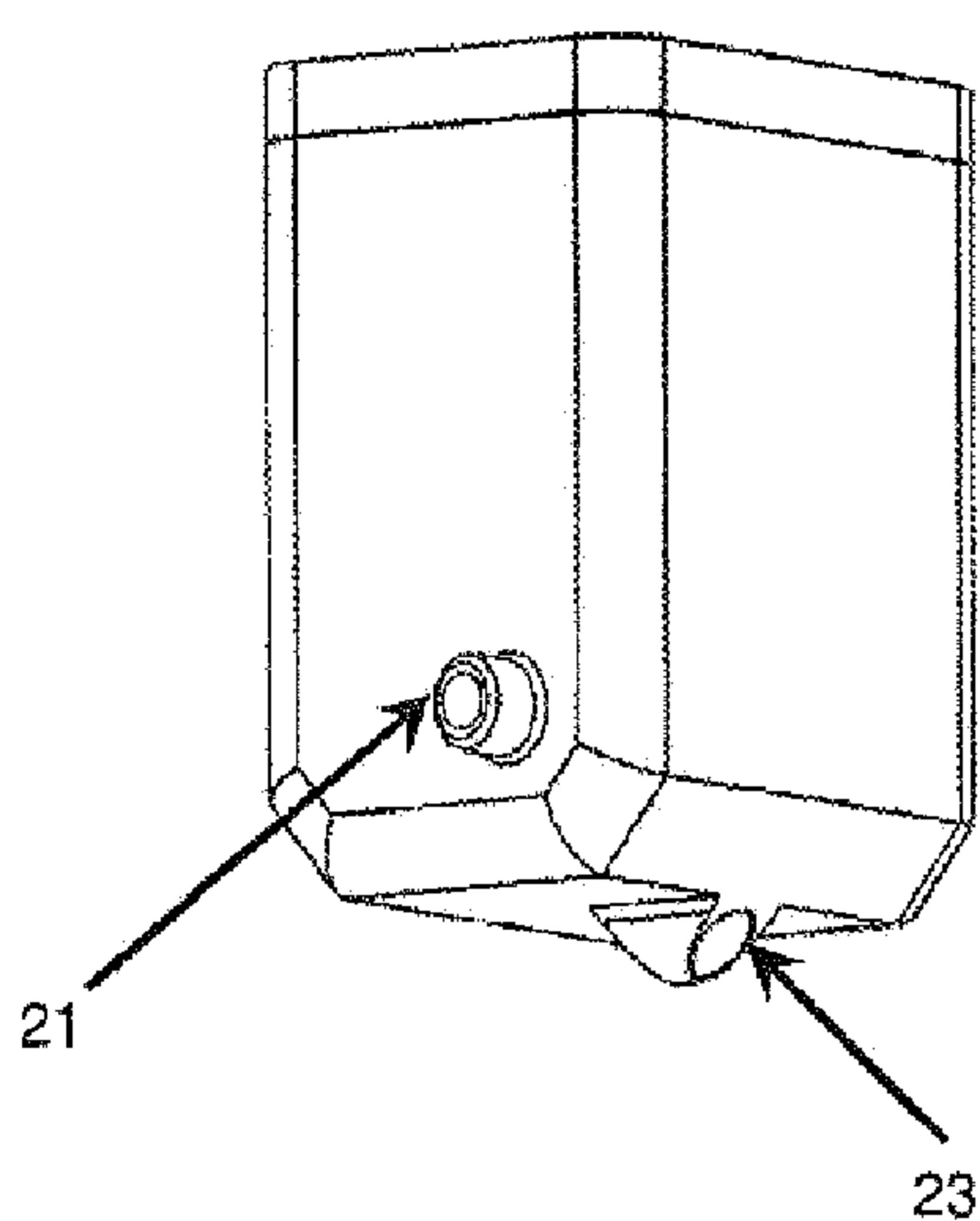


Fig. 8b

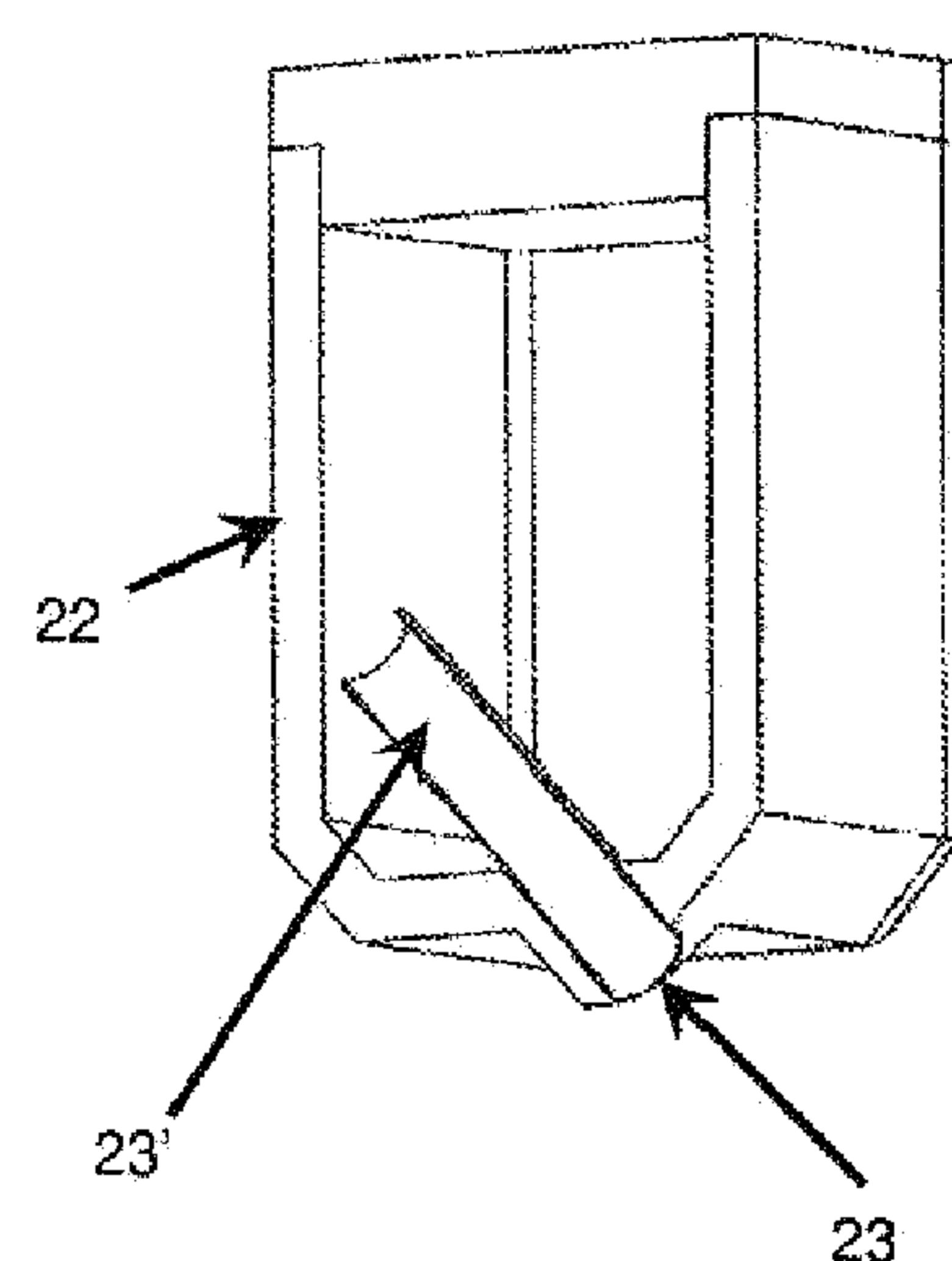


Fig. 9

