



(22) Date de dépôt/Filing Date: 1997/12/23

(41) Mise à la disp. pub./Open to Public Insp.: 1998/06/26

(45) Date de délivrance/Issue Date: 2009/10/13

(62) Demande originale/Original Application: 2 225 764

(30) Priorité/Priority: 1996/12/26 (US08/774,970)

(51) Cl.Int./Int.Cl. *B23K 37/04* (2006.01),
A61F 2/82 (2006.01), *C25F 3/16* (2006.01)

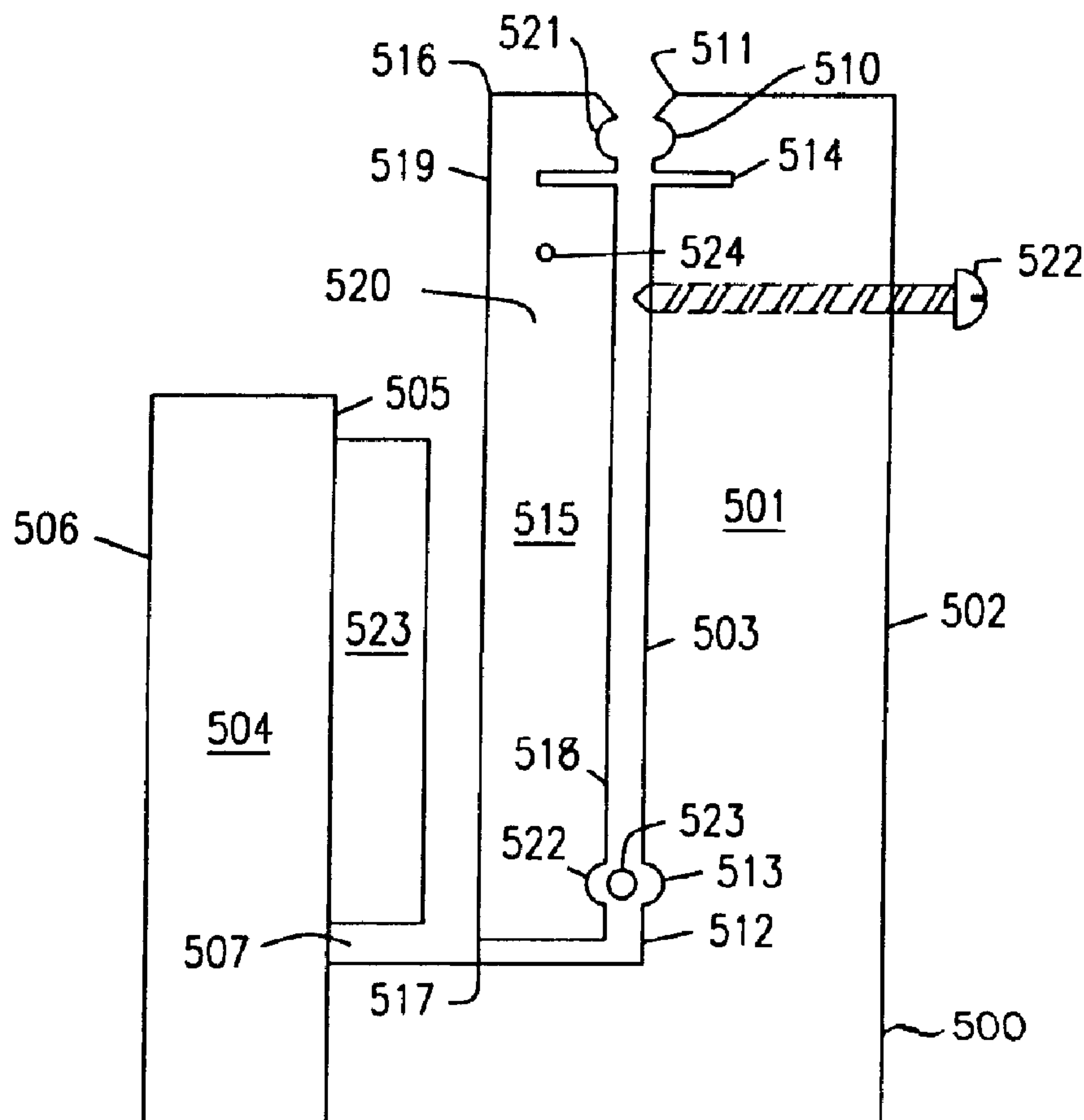
(72) Inventeur/Inventor:
RICHTER, JACOB, IL

(73) Propriétaire/Owner:
MEDINOL LTD., IL

(74) Agent: OGILVY RENAULT LLP/S.E.N.C.R.L.,S.R.L.

(54) Titre : METHODE DE FABRICATION D'UN TUTEUR ET APPAREIL

(54) Title: STENT FABRICATION METHOD AND APPARATUS



(57) Abrégé/Abstract:

A stent and a method for fabricating the stent are disclosed. The stent has an originally flat pattern and connection points where the sides of the flat pattern are joined. The method includes the steps of a) cutting a stent pattern into a flat piece of metal thereby to

(57) **Abrégé(suite)/Abstract(continued):**

produce a metal pattern, b) deforming the metal pattern so as to cause two opposing sides to meet, and c) joining the two opposing sides at least at one point. Substantially no portion of the stent projects into the lumen of the stent when the stent is expanded against the internal wall of a blood vessel.

ABSTRACT

A stent and a method for fabricating the stent are disclosed. The stent has an originally flat pattern and connection points where the sides of the flat pattern are joined. The method includes the steps of a) cutting a stent pattern into a flat piece of metal thereby to produce a metal pattern, b) deforming the metal pattern so as to cause two opposing sides to meet, and c) joining the two opposing sides at least at one point. Substantially no portion of the stent projects into the lumen of the stent when the stent is expanded against the internal wall of a blood vessel.

81786

5 STENT FABRICATION METHOD AND APPARATUS

10 FIELD OF THE INVENTION

The present invention relates generally to methods of fabricating stents.

BACKGROUND OF THE INVENTION

15 Stents are known in the art. They are typically formed of a cylindrical metal mesh which can expand when pressure is internally applied. Alternatively, they can be formed of wire wrapped into a cylindrical shape.

20 As described in U.S. 4,776,337 to Palmaz, the cylindrical metal mesh shape is produced by laser cutting a thin walled metal tube. The laser cuts away all but the lines and curves of the mesh.

25 The method of U.S. '337 is applicable for relatively large mesh shapes and for meshes whose lines are relatively wide. However, for more delicate and/or intricate shapes, the spot size of the laser is too large.

5

SUMMARY OF THE PRESENT INVENTION

It is, therefore, an object of the present invention to provide a stent fabrication method which can produce stents with relatively intricate and/or delicate designs.

10 The method involves first creating a flat version of the desired stent pattern from a piece of thin sheet metal. The flat pattern can be produced through any suitable technique, such as etching the design into the sheet metal, or by cutting with a very fine laser, should one become commercially available or by any other technique.

15 Once the sheet metal has been cut, it is deformed so as to cause its edges to meet. To create a cylindrical stent from a flat, roughly rectangular metal pattern, the flat metal is rolled until the edges meet. The locations where edges meet are joined together, such as by spot welding.

20 Afterwards, the stent is polished, either mechanically or electrochemically.

It is an object of this invention to provide an apparatus for fabricating a stent, comprising:

a) a platform adapted to receive a flat sheet of metal
25 to be formed into the stent, the flat sheet of metal having a longitudinal axis, a first major surface, a second major surface, a first long side, and a second long side, the first and the second long sides substantially parallel to the longitudinal axis of the sheet;

30 b) a mandrel having a substantially cylindrical external surface and having a first end and a second end defining a longitudinal axis, the mandrel sized to have a

5 cross-sectional diameter substantially equal to or less than
the internal diameter of the stent to be fabricated;

c) means for securing the mandrel against a major
surface of the flat sheet of metal; and

10 d) means for deforming the flat sheet of metal against
the external surface of the mandrel so that the flat sheet of
metal is deformed into a substantially tubular shape, the
means for deforming adapted so that the first long side and
the second long side remain substantially parallel to each
other when the flat sheet of metal is deformed into the
15 tubular shape.

It is another object of this invention to provide
and apparatus for fabricating a stent, comprising:

a) a base having a platform adapted to receive a flat
sheet of metal to be formed into the stent, the flat sheet of
20 metal having a longitudinal axis, a first major surface, a
second major surface, a first long side, and a second long
side, the first and the second long sides substantially
parallel to the longitudinal axis of the stent;

b) a mandrel having a substantially cylindrical
25 external surface and having a first end and a second end
defining a longitudinal axis, the mandrel sized to have a
cross-sectional diameter substantially equal to or less than
the internal diameter of the stent to be fabricated;

c) means for securing the mandrel against a major
30 surface of the flat sheet of metal;

d) a plurality of deforming blades disposed around the
periphery of the mandrel for deforming the flat sheet of metal

5 against the external surface of the mandrel so that the flat
sheet of metal is deformed into a substantially tubular shape,
the blades disposed between the first end and the second end
of the mandrel, each of the deforming blades adapted for
independent and selective movement in a first direction toward
10 the mandrel and a second direction away from the mandrel so as
to selectively impinge upon the mandrel or upon a portion of
the sheet disposed between the mandrel and each of the
deforming blades, each of the deforming blades further adapted
so that the first long side and the second long side of the
15 sheet remain substantially parallel to each other when the
stent is deformed into the tubular shape;

e) means for selectively moving each of the deforming
blades in a first direction toward the mandrel and in a second
direction away from the mandrel; and

20 f) means for securing the first long side of the sheet
to the second long side of the sheet.

It is yet another object of this invention to
provide an apparatus for fabricating a stent, comprising:
means for securing the first long side of the sheet to the
25 second long side of the sheet.

It is still another object of this invention to
provide an apparatus for fabricating a stent, comprising:

a) a base;

30 b) a sheet receiving area disposed on the base, the
area adapted to receive a flat sheet of metal to be formed
into the stent, the flat sheet of metal having a longitudinal
axis, a first major surface, a second major surface, a first

5 long side, and a second long side, the first and the second long sides substantially parallel to the longitudinal axis;

10 c) an arm having a first end and a second end, the first end of the arm adapted to selectively retain a mandrel having a substantially cylindrical external surface, the second end of the arm hingedly connected to the base and adapted for movement in a first direction toward the base and in a second direction away from the base and further adapted to secure the mandrel against a major surface of the flat sheet of metal disposed on the stent receiving area disposed
15 on the base, the mandrel sized to have a cross-sectional diameter substantially equal to or less than the internal cross-sectional diameter of the stent to be fabricated;

20 d) means for deforming the flat piece of metal against the external surface of the mandrel so that the flat sheet of metal is deformed into a substantially tubular shape substantially conforming to the external surface of the mandrel with the first long side and the second long side substantially parallel to each other.

25 It is yet another object of this invention to provide a stent aligning and welding jig comprising:

30 a) a base having a first end and a second end, a first wall having a first end and a second end and a first major surface and a second major surface; a second wall having a first end and a second end and a first major surface and a second major surface, the second major surface of the first wall and the first major surface of the second wall defining a longitudinal U-shaped channel having a longitudinal axis in

5 the base, the first wall provided with a plurality of slots
defining a plurality of first clamping portions having a top
end and a bottom end and a first major surface and a second
major surface, each of the first clamping portions provided
10 with a first concave channel disposed at the top end of the
second major surface of the first clamping portion and a
second concave channel disposed at the bottom end of the
second major surface of the first clamping portion, the first
and the second concave channels substantially parallel to the
longitudinal axis of the U-shaped channel; the first wall of
15 each of the plurality of first clamping portions provided with
a compensation slit disposed between the first concave channel
and the second concave channel, the compensation slit
substantially parallel to the longitudinal axis of the U-
shaped channel;

20 b) a plurality of second clamping portions disposed in
the U-shaped channel between the second major surface of the
first wall and the first major surface of the second wall,
each of the second clamping portions disposed in registry with
one of the first clamping portions, each of the second
25 clamping portions having a top end, a bottom end, a first
major surface, a second major surface, a first minor surface
disposed at the top end, a second minor surface disposed at
the bottom end, a third minor surface disposed between the top
end and the bottom end, and a fourth minor surface disposed
30 opposite the third minor surface between the top end and the
bottom end, each of the second clamping portions provided with
a first concave channel disposed at the top end of the first

5 major surface of the second clamping portion and a second concave channel disposed at the bottom end of the first major surface of the second clamping portion, the first and the second concave channels substantially parallel to the longitudinal axis of the U-shaped channel;

10 c) a biasing means disposed between the first major surface of the second wall and the second major surface of each of the plurality of second clamping portions for biasing the first major surface of each of the second clamping portions against the second major surface of each of the first
15 clamping portions which are in registry with each other;

d) a first mandrel support lever positioning pin projecting from the third minor surface and a second mandrel support lever positioning pin projecting from the fourth minor surface of each of the second clamping portions, the mandrel
20 support lever positioning pins substantially parallel to the longitudinal axis of the U-shaped channel;

e) a biasing control means for selectively controlling the distance between the second major surface of each of the first clamping portions and the first major surface of each of
25 the second clamping portions;

f) a retaining mandrel disposed in the second concave channel of the first wall and the second concave channel in each of the second clamping portions; and

g) a mandrel support lever for supporting the stent
30 during the alignment of the first long side of the sheet with the second long side of the sheet, the lever provided with a first mandrel support notch for supporting the first end of

5 the mandrel, a second mandrel support notch for supporting the
second end of the mandrel, a first mandrel support lever
positioning pin engagement surface for engaging the first
mandrel support lever positioning pin and a second mandrel
support lever positioning pin engagement surface for engaging
10 the second mandrel support lever positioning pin when the
mandrel support lever is disposed on the second wall.

It is still another object of this invention to
provide a method of fabricating a stent comprising the steps
of:

15 a) providing a plurality of stent patterns into a
flat piece of metal, each of the patterns having a first long
side and a second long side, the first long side provided with
a plurality of pairs of engagement points, the second long
side provided with a plurality of pairs of engagement points,
20 the plurality of pairs of engagement points disposed
substantially opposite each other, the engagement points sized
and disposed to communicate when the pattern is deformed and
rolled into a tubular shape, each pair of the first long side
engagement points provided with a bridge disposed between each
25 first long side engagement point comprising the pair, the
bridge having a width that is less than the width of the other
portions of the stent;

b) disposing a mandrel having a substantially
cylindrical external surface and a longitudinal axis between
30 the first long side and the second long side of the sheet, the
longitudinal axis substantially parallel to the first long
side and the second long side;

5 c) deforming the pattern into a tubular shape so
that the first long side pairs of engagement points contact
the second long side pairs of engagement points;

 d) cutting the bridge; and

 e) attaching each of the engagement points to the
10 engagement point with which it is in contact to form the
expandable stent.

 It is yet another object of this invention to
provide a jig for electropolishing a tubular stent,
comprising:

15 a) a base;

 b) an electrically conductive first member having a
first end connected to the base and a second end adapted to
selectively contact the external surface of the tubular stent
without damaging the external surface;

20 c) an electrically non-conductive second member having
a first end connected to the base and a second end adapted to
be selectively disposed within the longitudinal bore of the
stent without damaging the longitudinal bore, the first member
and the second member further adapted so as to bias the second
25 end of the second member towards the second end of the first
member in an amount sufficient to secure the stent between the
first and the second members.

 It is still another object to this invention to
provide a method of electropolishing a stent, comprising the
30 steps of:

 a) mounting a stent on a rack, the rack having a first
end and a second end provided with a plurality of stent

5 electropolishing mounts, each of the mounts having a base; an
electrically conductive first member having a first end
connected to the base and a second end adapted to selectively
contact the external surface of the tubular stent without
damaging the external surface; an electrically non-conductive
10 second member having a first end connected to the base and a
second end adapted to be selectively disposed within the
longitudinal bore of the stent without damaging the
longitudinal bore, the first member and the second member
further adapted so as to bias the second end of the second
15 member towards the second end of the first member in an amount
sufficient to secure the stent between the first and the
second members;

b) immersing the stent in an electropolishing bath and
applying electrical current to the first member for a
20 predetermined period of time; and

c) changing the point where the second end of the first
member contacts the external surface of the stent prior to the
expiration of the predetermined period of time.

It is yet another object of this invention to
25 provide a method of fabricating a stent comprising the steps
of:

a) providing a plurality of stent patterns in a
flat sheet of metal; each of the patterns having a first long
side and a second long side, the first long side provided with
30 a plurality of pairs of engagement points, the second long
side provided with a plurality of pairs of engagement points,
the plurality of pairs of engagement points disposed

5 substantially opposite each other, the engagement points sized
and disposed to communicate when the pattern is deformed and
rolled into a tubular shape, each pair of the first long side
engagement points provided with a bridge disposed between each
first long side engagement point comprising the pair, the
10 bridge having a width that is less than the width of the other
portions of the stent;

b) disposing a mandrel having a substantially
cylindrical external surface and a longitudinal axis between
the first long side and the second long side of the sheet, the
15 longitudinal axis substantially parallel to the first and the
second long sides;

c) deforming the pattern into a tubular shape so
that the first long side pairs of engagement points contact
the second long side pairs of engagement points and allowing a
20 portion of the stent to remain attached to the sheet of metal;

d) cutting the bridge;

e) attaching each of the engagement points to the
engagement point with which it is in contact to form the
stent;

25 f) attaching an electrode to the sheet of metal;

g) electropolishing the stent; and

f) disconnecting the stent from the sheet.

It is yet another object of this invention to provide a
sheet for fabricating a stent having a longitudinal lumen:

30 a) a flat piece of sheet metal provided with a
plurality of stent patterns, each of the patterns having a
first long side and a second long side, the first long side

5 provided with a plurality of pairs of engagement points, the
second long side provided with a plurality of pairs of
engagement points, the plurality of pairs of engagement points
disposed substantially opposite each other, the engagement
points sized and disposed to communicate when the pattern is
10 deformed and rolled into a tubular shape, each pair of the
first long side engagement points provided with a bridge
disposed between each first long side engagement point
comprising the pair, the bridge having a width that is less
than the width of the other portions of the stent.

15 It is yet another object of this invention to provide a
method for fabricating a stent having a longitudinal lumen
comprising the steps of:

a.) constructing an apparatus comprising:

- a) a laser housing;
- 20 b) a laser disposed within and selectively movable
within the housing;
- c) a movable table having a first end and a second end
and adapted for selective movement into and out of the laser
housing the table adapted so that when the first end of the
25 table is disposed within the laser housing the second end of
the table is disposed outside of the housing and when the
second end of the table is disposed within the laser housing
the first end of the table is disposed outside of the laser
housing;
- 30 d) a plurality of stent folders disposed at the first
end of the table and a plurality of stent folders disposed at
the second end of the table, each of the stent folders

5 comprising:

10 a) a base having a platform adapted to receive a flat sheet of metal to be formed into the stent, the flat sheet of metal having a longitudinal axis, a first major surface, a second major surface, a first long side, and a second long side, the first and the second long sides substantially parallel to the longitudinal axis, the sheet provided with a plurality of alignment of apertures;

15 b) a plurality of alignment pins projecting from each of the platforms, the pins sized to engage the alignment apertures and align the sheet on the platform;

20 c) a mandrel having a substantially cylindrical external surface and having a first end, a second end, and a longitudinal axis, the mandrel sized to have a cross-sectional diameter substantially equal to or less than the internal diameter of the stent to be fabricated, the platform provided with a first concave recess adapted to receive the first end of the mandrel and a second concave recess adapted to receive the second end of the
25 mandrel;

d) a hingedly connected arm adapted for movement in a first direction toward the platform and in a second direction away from the platform for securing the mandrel against a major surface of the flat sheet of metal;

30 e) a first deforming blade provided with a first deforming blade tip; a second deforming blade provided with a second deforming blade tip; a third deforming

5 blade provided with a third deforming blade tip; a fourth
deforming blade provided with a fourth deforming blade
tip; a fifth deforming blade provided with a fifth
deforming blade tip; and a sixth deforming blade provided
10 with a sixth deforming blade tip, the blades disposed
around the external surface of the mandrel, the deforming
blade tips adapted to deform the flat sheet of metal
against the external surface of the mandrel so that the
flat sheet of metal is deformed into a substantially
15 tubular shape substantially conforming to the external
surface, the deforming blades disposed between the first
end and the second end of the mandrel, each of the
deforming blades adapted for independent and selective
movement in a first direction toward the mandrel and a
20 second direction away from the mandrel so as to
selectively impinge the deforming blade tips against the
mandrel or against a portion of the sheet disposed
between the mandrel and each of the deforming blade tips,
each of the deforming blades further adapted so that the
first long side and the second long side of the sheet
25 remain substantially parallel to each other when the
stent is deformed into the tubular shape, the third and
the sixth deforming blade tips provided with a plurality
of scalloped laser apertures, the apertures sized and
disposed to permit the third and the sixth deforming
30 blade tips to secure the first long side and the second
long side against the external surface of the mandrel
while providing the laser access to predetermined

5 portions of the first long side and the second long side
of the sheet in order to weld the first long side to the
second long side;

10 f) a first motor connected to the first deforming
blade; a second motor connected to the second deforming
blade; a third motor connected to the third deforming
blade; a fourth motor connected to the fourth deforming
blade; a fifth motor connected to the fifth deforming
blade; and a sixth motor connected to the sixth deforming
blade, each of the motors adapted for selectively moving
15 each of the deforming blades to which it is connected in
a first direction toward the mandrel and in a second
direction away from the mandrel; and

20 g) a computer for controlling: the sequence which
the first end of the table and the second end of the
table are disposed within the laser housing; for
controlling the sequence and degree to which each of the
plurality of deforming blade tips impinges upon the
mandrel or a portion of the sheet disposed between the
mandrel and each of the deforming blade tips; and for
25 controlling the sequence, pattern, location, and amount
of energy the laser applies to each of the first and the
second long sides of each of the sheets disposed on each
of the plurality of stent folders;

30 b.) cutting a plurality of stent patterns into a flat piece
of metal, each of the patterns having a first major surface
and a second major surface, a first long side and a second

5 long side, the first long side provided with a plurality of
pairs of engagement points, the second long side provided with
a plurality of pairs of engagement points, the plurality of
pairs of engagement points disposed substantially opposite
each other, the engagement points sized and disposed to
10 communicate when the pattern is deformed and rolled into a
tubular shape, each pair of the first long side engagement
points provided with a bridge disposed between each first long
side engagement point comprising the pair, the bridge having a
width that is less than the width of the other portions of the
15 stent, the sheet provided with a plurality of alignment
apertures sized and disposed to engage the alignment pins on
the base;

c.) disposing the sheet on the base so that the first major
surface of the sheet is in contact with the base;

20 d.) disposing a mandrel having a substantially cylindrical
external surface and a longitudinal axis against the second
major surface of the sheet between the first long side and the
second long side of the sheet, the longitudinal axis
substantially parallel to the first long side and the second
25 long side;

e.) deforming the pattern into a tubular shape so that the
first long side pairs of engagement points contact the second
long side pairs of engagement points the deforming step
comprising the steps of:

30 a) actuating the sixth deforming blade motor so
that the sixth deforming blade motor moves the sixth
deforming blade in the first direction in an amount

5 sufficient for the sixth deforming blade tip to
contact the external surface of the mandrel so as to
secure the mandrel against the sheet;

10 b) actuating the first deforming blade motor so
that the first blade deforming motor moves the first
deforming blade in the first direction in an amount
sufficient for the first blade deforming tip to
contact the first major surface of the sheet and
deform the sheet against the external surface of the
mandrel;

15 c) actuating the second deforming blade motor so
that the second deforming blade motor moves the
second deforming blade in the first direction in an
amount sufficient for the second deforming blade tip
to contact the first major surface of the sheet and
20 deform the sheet against the external surface of the
mandrel;

25 d) actuating the third deforming blade motor so
that the third deforming blade motor moves the
second deforming blade in the first direction in an
amount sufficient for the third deforming blade tip
to contact the first major surface of the sheet and
deform the sheet against the external surface of the
mandrel while actuating the sixth deforming blade
motor so that the sixth deforming blade moves in the
25 second direction away from the mandrel;

30 e) actuating the fourth deforming blade motor so
that the fourth deforming blade motor moves the

- 5 fourth deforming blade tip in the first direction in
an amount sufficient for the fourth deforming blade
tip to contact the first major surface of the sheet
and deform the sheet against the external surface of
the mandrel;
- 10 f) actuating the fifth deforming blade motor so
that the fifth deforming blade motor moves the fifth
deforming blade in the first direction in an amount
sufficient for the fifth deforming blade tip to
contact the first major surface of the sheet and
15 deform the sheet against the external surface of the
mandrel;
- g) actuating the sixth deforming blade motor so
that the sixth deforming blade motor moves the
second deforming blade in the first direction in an
20 amount sufficient for the second deforming blade tip
to contact the first major surface of the sheet and
deform the sheet against the external surface of the
mandrel;
- h) simultaneously actuating the third and sixth
25 deforming blade motors so that the third and sixth
deforming blade motors move the third and sixth
deforming blades in the first direction in an amount
sufficient for the third and sixth deforming blade
tips to contact the first major surface of the sheet
30 and deform the sheet against the external surface of
the mandrel;
- d) utilizing the laser in cutting the bridge; and

5 e) utilizing the laser in welding each of the engagement points to the engagement point with which it is in contact to form the expandable stent.

It is a further object of this invention to provide a stent having a longitudinal lumen, comprising: a first long
10 side and a second long side, the first long side provided with a plurality of pairs of engagement points, the second long side provided with a plurality of pairs of engagement points, the plurality of pairs of first long side engagement points and the plurality of pairs of second long side engagement
15 points disposed substantially opposite each other and connected to each other via a weld, the weld wider than the other portions of the stent.

20

5 BRIEF DESCRIPTION OF THE DRAWINGS

The present invention will be understood and appreciated more fully from the following detailed description taken in conjunction with the drawings in which:

10 Fig. 1 is a flow chart illustration of the stent fabrication method of the present invention;

Figs. 2A, 2B and 2C are illustrations of three alternative stent patterns to be etched, in accordance with the method of Fig. 1, into a flat sheet of metal;

15 Fig. 3 is an isometric illustration of a stent being deformed, useful in understanding the method of Fig. 1;

Fig. 4 is an isometric illustration of a stent formed from the method of Fig. 1;

Figs. 5A and 5B are side and top view illustrations, respectively, of one connection location of the stent of Fig. 4;
20 Fig. 6 is a side view illustration of one connection location of the stent of Fig. 4 which is connected in a nail-like manner;

Fig. 7 shows a piece of sheet metal with a plurality of patterns made in accordance with the invention;

25 Fig. 8 shows a detailed view of one of the patterns shown in Fig. 7;

Fig. 9 shows a detailed view of a pair of engagement troughs shown in Fig. 8;

30 Fig. 10 shows a detailed view of a pair of engaging protrusions shown in Fig. 8;

Fig. 11 shows the engagement troughs and engagement protrusions of Figs. 9 and 10 in the engaged position;

5 Fig. 12 shows a welding run practiced in accordance
with the invention;

 Fig. 13 is a detailed view of the welding run shown
in Fig. 12;

 Fig. 14 is a detailed view of a cell of a stent made
10 in accordance with this invention;

 Fig. 15 is a detailed view of a cell made in
accordance with this invention;

 Fig. 16 shows a cell of a stent made in accordance
with this invention;

15 Fig. 17 is an enlarged view of the cell shown in
Fig. 16;

 Fig. 18 is a cross-sectional view of a longitudinal
member of a stent constructed in accordance with this
invention;

20 Fig. 19 is a cross-sectional view of a stent
constructed in accordance with this invention;

 Fig. 20 is a perspective view of a stent constructed
in accordance with this invention;

 Fig. 21 is a cross-sectional front view of an
25 unexpanded stent made in accordance with the invention;

 Fig. 22 is a cross-sectional front view of the stent
shown in Fig. 21 after it has been expanded;

 Fig. 23 is a cross-sectional front view of an
unexpanded stent made by cutting a pattern in a tube; and

30 Fig. 24 is a cross-sectional front view of the stent
shown in Fig. 23 after expansion;

 Fig. 25 shows an apparatus for constructing a stent

5 made in accordance with the invention;

Fig. 26 shows an apparatus for constructing a stent made in accordance with the invention;

Fig. 27 is an enlarged view of a portion of the apparatus shown in FIG. 26;

10 Fig. 28 shows engagement points constructed in accordance with the invention;

Fig. 29 show engagement points constructed in accordance with the invention;

15 Fig. 30A to 30I shows the sequence of making a stent using the apparatus of FIGS. 25 and 26;

Fig. 31 shows details of a v-shaped notch and gap formed in accordance with the invention;

Fig. 32 shows details of two blade deforming tips made in accordance with the invention;

20 Fig. 33 shows an alternative embodiment of engagement of engagement points constructed in accordance with the invention;

Fig. 34 shows an alternative embodiment of engagement points constructed in accordance with the invention;

Fig. 35 shows a mandrel utilized in accordance with the invention;

Fig. 36 shows a mandrel receiving surface made in accordance with the invention;

30 Fig. 37 shows an alternative embodiment of an apparatus constructed in accordance with the invention;

Fig. 38 is a top view of FIG. 37.;

5 Fig. 39 shows a means for deforming a stent made in accordance with the embodiment shown in FIGS. 37 and 38;

 Fig. 40 is a side view of the deforming means shown in FIG. 39;

 Fig. 41 shows a stent aligning and welding jig
10 constructed in accordance with the invention;

 Fig. 42 shows a mandrel support lever;

 Fig. 43 is a front view of the jig shown in FIG. 41;

 Fig. 44 is a top view of the jig shown in FIG. 43;

 Fig. 45 shows the mandrel support lever of FIG. 42
15 disposed on the jig of FIG. 41;

 Fig. 46 shows a mount for electropolishing a stent;

 Fig. 47 shows the mount of FIG. 46 with the stent moved in a longitudinal direction;

 Fig. 48 shows a rack for electropolishing a stent
20 with material to be sacrificed disposed at the ends;

 Fig. 49 shows a stent still attached to a metal sheet for electropolishing by attaching an electrode to the sheet; and

 Fig. 50 is a side view of FIG. 49 showing the stent
25 and the remaining portion of the sheet.

DETAILED DESCRIPTION OF A PREFERRED EMBODIMENT

 Reference is now made to Fig. 1, which illustrates
30 the stent fabrication method of the present invention and to Figs. 2A, 2B, 2C, 3 and 4 which are useful in understanding the method of Fig. 1.

5 In the stent fabrication method of the present invention, a stent designer first prepares a drawing of the desired stent pattern in a flat format (step 10).

 Figs. 2A, 2B and 2C illustrate three exemplary stent pattern designs. The pattern of Fig. 2A has two types of
10 sections 20 and 22. Each section 20 has two opposing periodic patterns and each section 22 has a plurality of connecting lines 24. The pattern of Fig. 2A can be formed of any size; a preferable size is to have each section 20 be between 1 and
15 6mm wide and each section 22 have connecting lines 24 of 1 - 6mm long. At such sizes, the pattern of Fig. 2A cannot be cut using a laser cutting system.

 The pattern of Fig. 2B is similar to that of Fig. 2A in that it also has sections 20 of opposing periodic patterns. The pattern of Fig. 2B also has connecting
20 sections, labeled 30, which have a Z shape.

 The pattern of Fig. 2C has no connecting sections. Instead, it has a series of alternating patterns, labeled 32 and 34.

 The patterns of Figs. 2A, 2B and 2C optionally also
25 have a plurality of small protrusions 38 which are useful in forming the stent, as described hereinbelow.

 Returning to Fig. 1, in step 12, the stent pattern is cut into a flat piece of metal ("sheet metal"). The metal can be any type of biocompatible material, such as stainless
30 steel, or a material which is plated with a biocompatible material. The cutting operation can be implemented in any of a number of ways, such as by etching, or by cutting with a

5 fine cutting tool, or by cutting with a very fine laser,
should one become commercially available.

If step 12 is implemented with etching, then, the
process is designed to cut through the sheet metal. This
process is known; however, for the purposes of completeness,
10 it will be briefly described hereinbelow.

The drawing of the pattern is reduced and printed
onto a transparent film. Since it is desired to cut
completely through the metal, the drawing is printed onto two
films which are joined together in a few places along their
15 edges. The sheet metal is covered, on both sides, with a
layer of photoresist and placed between the two transparent,
printed films. The structure is illuminated on both sides
which causes the portions of the photoresist which receive the
light (which are all the empty spaces in the pattern, such as
20 spaces 26 of Fig. 2A) to change properties.

The sheet metal is placed into acid which eats away
those portions of the photoresist which changes properties.
The sheet metal is then placed into an etching solution which
etches
25 away all material on which there is no photoresist-removing
solution which removes the photoresist, leaving the metal
having the desired stent pattern.

In step 14, the metal pattern is deformed so as to
cause its long sides (labeled 28 in Figs. 2A, 2B and 2C) to
30 meet each other. Fig. 3 illustrates the deformation process.
For cylindrical stents, the deformation process is a rolling
process, as shown.

5 If the protrusions 38 have been produced, after deformation of the metal pattern, the protrusions 38 protrude over the edge 28 to which they are not attached. This is illustrated in Fig. 5A.

10 In step 16, the edges 28 are joined together by any suitable process, such as spot welding. If the protrusions 38 were made, the protrusions 38 are joined to the opposite edge 28, either by welding, adhesive or, as illustrated in Fig. 6, with a nail-like element 40. Fig. 5B illustrates the connection of the protrusion to the opposite edge 28. Since
15 protrusion 38 is typically designed to extend the width of one loop 39, the pattern is approximately preserved. This is seen in Fig. 5B.

 Alternatively, the edges 28 can be brought together and joined in the appropriate places.

20 Fig. 4 illustrates a stent 31 formed by the process of steps 10 - 16 for the pattern of Fig. 2A. It is noted that such a stent has connection points 32 formed by the joining of the points 30.

 Finally, the stent 31 is polished to remove any
25 excess material not properly removed by the cutting process (step 12). The polishing can be performed mechanically, by rubbing a polishing stick having diamond dust on its outside inside the stent 31. Alternatively, an electropolishing unit can be utilized.

30 Fig. 7 shows an alternative embodiment of the invention in which a plurality of patterns 120 are etched and cut into the sheet metal 121 as previously discussed. Fig. 8 is an enlarged view of one of the plurality of patterns 120

5 shown in Fig. 7.

Fig. 9 is an enlarged view of one pair 127 of the plurality of engagement troughs 128 and 129 shown in Fig. 8. Fig. 10 is an enlarged view of one pair 130 of the plurality of engagement protrusions 131 and 132 shown in Fig. 8. The
10 sheet metal 121 and each of the patterns 120 is provided with a plurality of alignment apertures 122 and 122' adapted to receive sprockets (not shown) for precisely moving and maintaining the precise alignment of the sheet metal 121 and the patterns 120 during the various stages of manufacturing.
15 Each pattern 120 has a first long side 123 and a second long side 124, a first short side 125, and a second short side 126. The first long side 123 is provided with a plurality of pairs 127, 127' and 127" of engagement troughs 128 and 129 (shown in greater detail in Fig. 9). Each pair 127, 127' and 127" of
20 engagement troughs has a first engagement trough 128 and a second engagement trough 129. The second long side 124 is provided with a plurality of pairs 130, 130' and 130" of engagement protrusions (shown in greater detail in Fig. 10). Each pair 130, 130' and 130" of engagement protrusions is
25 provided with a first engagement protrusion 131 and a second engagement protrusion 132. The pairs of engagement protrusions 130, 130' and 130" are disposed substantially opposite the pairs of engagement troughs 127, 127' and 127".

The engagement troughs 128 and 129 are disposed and
30 adapted to receive and engage the engagement protrusions 131 and 132 so that the alignment of the stent is maintained when the pattern 120 is deformed and the flat sheet metal is rolled

5 so that the first long side 123 and the second long side 124
meet each other to form a tube as shown in Figs. 19 and 20.

 A bridge 133 of material is disposed between each
pair 127, 127' and 127" of engagement troughs 128 and 129.
This bridge 133 imparts additional stability and facilitates
10 alignment during manufacturing and imparts additional strength
to the welds of the finished stent as discussed below.

 After the sheet has been rolled into a tubular stent
and the engagement troughs 128 and 129 have received the
engagement protrusions 131 and 132, means (not shown) are
15 utilized to maintain the alignment and the bridge 133 is cut
to leave two substantially equal parts. The bridge 133 may be
cut in a variety of ways well known to those skilled in the
art, however, in a preferred embodiment, a laser is utilized.
Engagement trough 128 is welded to engagement protrusion 131
20 and engagement trough 129 is welded to engagement protrusion
132 as shown in Figs. 12 and 13. This may be accomplished in
a variety of ways well known to those skilled in the art,
however, in a preferred embodiment a plurality of spot welds
are utilized. In an especially preferred embodiment, about
25 five spot welds are used in each weld run as shown in Figs. 12
and 13. The heat produced by the welding melts the cut bridge
133 material and the material is drawn towards the engagement
trough 128 or 129 to which the material is attached and is
drawn into the welded area between the engagement trough and
30 the engagement protrusion where the additional bridge material
becomes part of and imparts additional strength to the weld.
The stent may then be finished as previously discussed.

5 Fig. 13 is an enlarged view of the welded area shown in Fig. 12. In a preferred embodiment, the weld run is offset from the point where the engagement trough and the engagement protrusion contact each other. In an especially preferred embodiment, the weld run is offset about .01 mm.

10 Fig. 14 is a detailed view of the pattern shown in Fig. 8. As shown in Figs. 14 and 20, Applicants' invention can also be described as an expandable stent defining a longitudinal aperture 80 having a longitudinal axis or extension 79 and a circumferential axis or extension 105, including a plurality of flexible connected cells 50 with each of the flexible cells 50 having a first longitudinal end 77 and a second longitudinal end 78. Each cell 50 also is provided with a first longitudinal apex 100 disposed at the first longitudinal end 77 and a second longitudinal apex 104 disposed at the second longitudinal end 78. Each cell 50 also includes a first member 51 having a longitudinal component having a first end 52 and a second end 53; a second member 54 having a longitudinal component having a first end 55 and a second end 56; a third member 57 having a longitudinal component having a first end 58 and a second end 59; and a fourth member 60 having a longitudinal component having a first end 61 and a second end 62. The stent also includes a first loop 63 defining a first angle 64 disposed between the first end 52 of the first member 51 and the first end 55 of the second member 54. A second loop 65 defining a second angle 66 is disposed between the second end 59 of the third member 57 and the second end 62 of the fourth member 60 and is

5 disposed generally opposite to the first loop 63. A first flexible compensating member or flexible link 67 having a first end 68 and a second end 69 is disposed between the first member 51 and the third member 57 with the first end 68 of the first flexible compensating member or flexible link 67 communicating with the second end 53 of the first member 51 and the second end 69 of the first flexible compensating member or flexible link 67 communicating with the first end 58 of the third member 57. The first end 68 and the second end 69 are disposed a variable longitudinal distance 70 from each other. A second flexible compensating member 71 having a first end 72 and a second end 73 is disposed between the second member 54 and the fourth member 60. The first end 72 of the second flexible compensating member or flexible link 71 communicates with the second end 56 of the second member 54 and the second end 73 of the second flexible compensating member or flexible link 71 communicates with the first end 61 of the fourth member 60. The first end 72 and the second end 73 are disposed a variable longitudinal distance 74 from each other. In a preferred embodiment, the first and second flexible compensating member or flexible links 67 and 71 are arcuate. The first and second flexible compensating member or flexible links 67 and 71 are differentially extendable or compressible when the stent is bent in a curved direction away from the longitudinal axis 79 of the aperture 80. (Shown in Fig. 20.) The first member 51, second member 54, third member 57, and fourth member 60 and the first loop 63 and the second loop 65 and the first flexible compensating member or flexible

5 link 67 and the second flexible compensating member or
flexible link 71 are disposed so that as the stent is expanded
the distance between the first flexible compensating member or
flexible link 67 and the second flexible compensating member
or flexible link 71 increases and the longitudinal component
10 of the first member 51, second member 54, third member 57 and
fourth member 60 decreases while the first loop 63 and the
second loop 65 remain generally opposite to one another, the
ends 68 and 69 of the first flexible compensating member or
flexible link 67 and the ends 72 and 73 of the second flexible
15 compensating member or flexible link 71 open so as to increase
the variable longitudinal distance 70 between the first end 68
and the second end 69 of the first flexible compensating
member or flexible link 67 and so as to increase the variable
longitudinal distance 74 between the first end 72 and the
20 second end 73 of the second flexible compensating member or
flexible link 71. This compensates for the decreasing of the
longitudinal component of the first member 51, second member
54, third member 57, and fourth member 60 and substantially
lessens the foreshortening of the stent upon its expansion.
25 Upon expansion, the first flexible compensating member 67 and
the second flexible compensating member 71 impart support to
the lumen being treated.

Fig. 15 shows the dimensions of an especially
preferred embodiment of this invention. The deflection
30 points, i.e., the first and second loops 63 and 65 and the
first and second compensating members 67 and 71, are made
wider than the first, second, third, and fourth members 51,

5 54, 57 and 60 so that the force of the deflection is
distributed over a wider area upon the expansion of the stent.
The deflection points can be made wider than the first,
second, third and fourth members in differing amounts so that
the deflection will occur in the narrower areas first due to
10 the decreased resistance. In a preferred embodiment, the
first and second compensating members are wider than the
first, second, third and fourth members and the first and
second loops are wider than the first and second compensating
members. One of the advantages of sizing the first and second
15 loops so that they are wider than the first and second
compensating members is that the stent will substantially
compensate for foreshortening as the stent is expanded. In
the embodiment shown in Fig. 15, the first, second, third and
fourth members 51, 54, 57 and 60 have a width of about 0.1 mm.
20 The first and second loops 63 and 65 have a width of about
0.14 mm. The first and second compensating members 67 and 71
are provided with a thickened portion 75 and 76 having a width
of about 0.12 mm. Thus, in this especially preferred
embodiment, the first and second loops have a width that is
25 about 40% greater and the first and second compensating
members have a width that is about 20% greater than the width
of the first, second, third and fourth members.

Figs. 16 through 20 show details of a stent
constructed in accordance with this invention.

30 Yet another advantage of Applicant's invention is
shown in Figs. 21 to 24. For the sake of clarity, the
dimensions and the degree of displacement of the components of

5 the stents shown in Figs. 21 to 24 has been intentionally exaggerated.

Fig. 21 is a cross-sectional front view taken along line A-A of the unexpanded stent made in accordance with applicants invention shown in Fig. 20. The unexpanded stent 10 200 of Fig. 21 is shown disposed in the lumen 202 of a blood vessel 201 prior to expansion. As previously discussed, this stent is made by first cutting the stent pattern into a flat piece of sheet metal and then rolling the sheet metal into a tube to form the tubular stent. As shown in Fig. 21 after 15 rolling, the first and second flexible compensating members 67 and 71 of the unexpanded stent tend to "flare out" in a direction away from the longitudinal axis or lumen of the stent. Thus, the flexible compensating members 67 and 71 define outer diameters which are larger than the outer 20 diameters defined by the remaining portions of the stent. Fig. 22 shows the stent of Fig. 21 after it has been expanded in the lumen and against the internal wall of the blood vessel. As shown in Fig. 22, upon expansion of the unexpanded stent toward the wall of the blood vessels, the walls of the 25 blood vessel imparts a mechanical force to the first and second flexible compensating members 67 and 71 and the compensating members move toward the longitudinal axis or lumen of the stent until they are substantially in registry with the remaining portion of the stent. Thus, the lumen of 30 the expanded stent is substantially circular when viewed in cross section with substantially no portion of the expanded stent projecting into the lumen or towards the longitudinal

5 axis of the expanded stent.

Fig. 23 is similar to Fig. 21 except that the pattern has been cut into a tubular member using conventional methods of making stents. As shown in Fig. 23, the flexible compensating members do not flare out away from the longitudinal axis of the unexpanded stent 203. Upon the expansion of the stent shown in Fig. 23 toward the walls of the blood vessel 201, the flexible compensating members 67' and 71' tend to "flare in" and project into the lumen 204 of the expanded stent 203.

15 Fig. 24 shows the stent 203 of Fig. 23 after it has been expanded in a lumen 204 of a blood vessel 201. The flexible compensating members 67' and 71' are not in registry with the remaining portions of the stent and define a diameter smaller than the diameter of remaining portions of the stent. These projections into the lumen of the stent create turbulence in a fluid flowing through the longitudinal axis of the expanded stent and could result in clot formation.

20 Applicant's invention is also directed to an apparatus for fabricating a stent, comprising a platform, a mandrel, and means for deforming a sheet of metal around the mandrel.

The platform is adapted to receive a flat sheet of metal to be formed into a stent. In a preferred embodiment, the flat sheet of metal is provided with a first end, a second end defining a longitudinal axis, a first major surface, a second major surface, a first long side, a second long side, with the first and said second long sides substantially

5 parallel to the longitudinal axis of the sheet. The mandrel
has a substantially cylindrical external surface and a first
end and a second end defining a longitudinal axis. The
mandrel is sized to have a cross-sectional diameter
substantially equal to or less than the internal diameter of a
10 stent to be fabricated. A means for securing the mandrel
against a major surface of the flat sheet of metal is
provided. A means for deforming the flat sheet of metal
around the external surface of the mandrel is also provided to
deform the flat sheet of metal into a substantially tubular
15 shape that substantially conforms to the external surface of
the mandrel. In a preferred embodiment, the means for
deforming the sheet is adapted so that the first long side and
the second long side remain substantially parallel to each
other when the flat sheet of metal is deformed into a tubular
20 shape. A means, e.g., a welding apparatus, laser, adhesive,
or screw secures the first long side of the sheet to the
second long side of the sheet.

In operation of a preferred embodiment a plurality
of stent patterns are cut or etched into a flat piece of
25 metal. Each of the patterns has a first long side and a
second long side, with the first long side provided with a
plurality of pairs of engagement points and second long side
provided with a plurality of pairs of engagement points. The
plurality of pairs of engagement points are disposed
30 substantially opposite each other and are sized and disposed
to communicate when the pattern is deformed and rolled into a
tubular shape. Each pair of the first long side engagement

5 points is provided with a bridge disposed between each first long side engagement point comprising the pair, the bridge having a width that is less than the width of the other portions of the stent.

10 A mandrel is disposed between the first and second long sides of the sheet. The mandrel has a substantially cylindrical external surface and a longitudinal axis substantially parallel to the first long side and the second long sides. The pattern is deformed into a tubular shape so that the first long side pairs of engagement points contact
15 the second long side pairs of engagement points.

The bridge is cut and each of the engagement points is attached to the engagement point with which it is in contact to form the expandable stent.

20 Figs. 25 to 28 show a preferred embodiment of an apparatus for fabricating and a stent constructed in accordance with Applicants' invention. The apparatus comprises a laser housing 300, a laser 301, a movable table 302, and a plurality of stent folders 303 disposed on the table. The laser 301 is disposed within and selectively
25 movable within the housing 300. The movable table 302 has a first end 304 and a second end 305 and is adapted for selective movement into and out of the laser housing 300. The table 302 is adapted so that when the first end 304 of the table 302 is disposed within the laser housing 300 the second
30 end of the table 305 is disposed outside of said housing 300 and when said second end 305 of the table 302 is disposed within the laser housing 300 the first end 304 of the table

5 302 is disposed outside of the laser housing 300.

A plurality of stent folders 303 is disposed at the first end 304 of the table and a plurality of stent folders 303 is disposed at the second end 305 of the table 302. As shown in FIGS. 26 and 27, each of said stent folders
10 comprises:

A base 306 having a platform 307 adapted to receive a flat sheet of metal 120 to be formed into a stent. The flat sheet of metal 120 has a longitudinal axis, a first major surface, a second major surface, a first long side,
15 and a second long side, with the first and the second long sides substantially parallel to the longitudinal axis. The sheet is also provided with a plurality of alignment of apertures 122.

A plurality of alignment pins 308 project from each
20 of the platforms. The pins 308 are sized to engage the alignment apertures 122 and align the sheet on the platform 307.

A mandrel 309 is provided having a substantially cylindrical external surface 310 and having a first end
25 311, a second end 312, and a longitudinal axis 313 as shown in FIGS. 35. The mandrel 309 is sized to have a cross-sectional diameter D substantially equal to or less than the internal diameter of the stent to be fabricated. The platform 307 is provided with a first concave recess
30 314 adapted to receive the first end 311 of the mandrel and a second concave recess 315 adapted to receive the second end 312 of the mandrel 309 as shown in FIG. 36.

5 A hingedly connected arm 376 is adapted for movement
in a first direction toward the platform 307 and in a
second direction away from the platform 307 for securing
the mandrel 309 against a major surface of said flat
sheet of metal when it is disposed on the platform.

10 Each stent folder 303 is provided with a first
deforming blade 316 provided with a first deforming blade
tip 316'; a second deforming blade 317 provided with a
second deforming blade tip 317'; a third deforming blade
318 provided with a third deforming blade tip 318'; a
15 fourth deforming blade 319 provided with a fourth
deforming blade tip 319'; a fifth deforming blade 320
provided with a fifth deforming blade tip 320'; and a
sixth deforming blade 321 provided with a sixth deforming
blade tip 321'. The blades are disposed around the
20 external surface 310 of the mandrel 309 and are adapted
to deform the flat sheet of metal against the external
surface 310 of the mandrel 309 so that the flat sheet of
metal is deformed into a substantially tubular shape
substantially conforming to the external surface 310 of
25 the mandrel 309. The deforming blades are disposed
between the first end 311 and the second end 312 of the
mandrel 309. Each of the deforming blades is adapted for
independent and selective movement in a first direction
toward the mandrel 309 and a second direction away from
30 the mandrel so as to selectively impinge the deforming
blade tips 316', 317', 318', 319', 320', and 321' against
the mandrel or against a portion of the sheet disposed

5 between the mandrel and each of the deforming blade tips.
Each of the deforming blades is also adapted so that the
first long side and the second long side of the sheet
remain substantially parallel to each other when the
sheet is deformed into the tubular shape. The third and
10 the sixth deforming blade tips 318' and 321' are provided
with a plurality of scalloped laser apertures 322, as
shown in FIG. 32, which are sized and disposed to permit
the third and the sixth deforming blade tips to secure
the first long side and the second long side against the
15 external surface of the mandrel while providing the laser
301 access to predetermined portions of the first long
side and the second long side of the sheet in order to
weld the first long side to the second long side.

A first motor 323 is connected to the first
20 deforming blade; a second motor 324 is connected to the
second deforming blade; a third motor 325 is connected to
the third deforming blade; a fourth motor 326 is
connected to the fourth deforming blade; a fifth motor
327 is connected to the fifth deforming blade; and a
25 sixth motor 328 is connected to the sixth deforming
blade. Each of the motors is adapted for selectively
moving each of the deforming blades to which it is
connected in a first direction toward the mandrel and in
a second direction away from the mandrel.

30 A computer 329 controls the sequence which the first
end of the table and the second end of the table are
disposed within the laser housing; the sequence and

5 degree to which each of the deforming blade tips impinges
upon the mandrel or a portion of the sheet disposed
between the mandrel and each of the deforming blade tips;
and the sequence, pattern, location, and amount of energy
the laser applies to each of the first and second long
10 sides of each of the sheets disposed on each of the
plurality of stent folders.

Each of the blade deforming tips has a length
substantially equal to the first and the second long sides of
the flat sheet of metal and in a preferred embodiment the
15 blade deforming tips are concave as shown in FIG. 27.

In an especially preferred embodiment, as shown in
FIG. 27 the third deforming blade tip is substantially
identical to the sixth deforming blade tip; the second
20 deforming blade tip is substantially identical to the fifth
deforming blade tip; and the first deforming blade tip is
substantially identical to the fourth deforming blade tip.

In operation, the apparatus shown in FIGS. 25 to 27
and discussed in detail above is constructed. A plurality of
25 stent patterns is cut into a flat piece of metal, each of the
patterns having a first major surface and a second major
surface, a first long side and a second long side. The first
long side and the second long sides are provided with a
plurality of pairs of engagement points 329, 330, 331, and
30 332, as shown in FIGS. 28 and 29, disposed substantially
opposite each other and sized and disposed to communicate when
the pattern is deformed and rolled into a tubular shape. Each

5 pair of the first long side engagement points is provided with
a bridge 333 disposed between each first long side engagement
point 329 and 330 comprising the pair. Preferably, the bridge
333 has a width that is less than the width of the other
portions of the stent. The sheet is also provided with a
10 plurality of alignment apertures 122 sized and disposed to
engage the alignment pins 308 on the base 306.

The sheet is disposed on the base so that the first
major surface of the sheet is in contact with the base.

A mandrel 309 having a substantially cylindrical
15 external surface 310 and a longitudinal axis 313 is disposed
against the second major surface of the sheet between the
first long side and the second long side of the sheet with the
longitudinal axis substantially parallel to the first long
side and the second long side, as shown in FIG 30A.

20 The pattern is deformed into a tubular shape so that
the first long side pairs of engagement points contact the
second long side pairs of engagement points, as shown in FIG.
29. The deforming step comprises the steps of:

a) actuating the sixth deforming blade motor so
25 that the sixth deforming blade motor moves the sixth
deforming blade in the first direction in an amount
sufficient for the sixth deforming blade tip to
contact the external surface of the mandrel so as to
secure the mandrel against said sheet, as shown in
30 FIG. 30B.

The first deforming blade motor is activated so
that the first blade deforming motor moves the first

5 deforming blade in the first direction in an amount
sufficient for the first blade deforming tip to
contact the first major surface of the sheet and
deform the sheet against the external surface of the
mandrel, as shown in FIG. 30C.

10 The second deforming blade motor is then
activated so that the second deforming blade motor
moves the second deforming blade in the first
direction in an amount sufficient for the second
deforming blade tip to contact the first major
15 surface of the sheet and deform the sheet against
the external surface of the mandrel, as shown in
FIG. 30D.

 The third deforming blade motor is then
activated so that the third deforming blade motor
20 moves the second deforming blade in the first
direction in an amount sufficient for the third
deforming blade tip to contact the first major
surface of the sheet and deform the sheet against
the external surface of the mandrel while actuating
25 the sixth deforming blade motor so that the sixth
deforming blade moves in the second direction away
from said mandrel, as shown in FIG. 30E.

 The fourth deforming blade motor is then
activated so that the fourth deforming blade motor
30 moves the fourth deforming blade tip in the first
direction in an amount sufficient for the fourth
deforming blade tip to contact the first major

5 surface of the sheet and deform the sheet against
the external surface of the mandrel, as shown in
FIG. 30F.

The fifth deforming blade motor is then
activated so that the fifth deforming blade motor
10 moves the fifth deforming blade in the first
direction in an amount sufficient for the fifth
deforming blade tip to contact the first major
surface of the sheet and deform the sheet against
the external surface of the mandrel, as shown in
15 FIG. 30G.

The sixth deforming blade motor is then
activated so that the sixth deforming blade motor
moves the sixth deforming blade in the first
direction in an amount sufficient for the sixth
20 deforming blade tip to contact the first major
surface of the sheet and deform the sheet against
the external surface of the mandrel, as shown in
Fig. 30H.

The third and sixth deforming blade motors are
25 then simultaneously activated so that the third and
sixth deforming blade motors move the third and
sixth deforming blades in the first direction in an
amount sufficient for the third and sixth deforming
blade tips to contact the first major surface of the
30 sheet and deform the sheet against the external
surface of the mandrel as shown in FIG. 30I.

The laser is used to cut the bridge. The laser is then

5 used to weld each of the engagement points to the engagement point with which it is in contact to form the expandable stent.

In a preferred embodiment, the bridge has a width that is about 25% to about 50% of the width of the other portions of the stent and in an especially preferred embodiment the bridge has a width of about 40 microns.

The engagement points, as shown in FIGS. 28 and 29 are sized and adapted to move in an amount sufficient so as to reduce the likelihood of material stress occurring during welding heating and cooling cycles.

A V-shaped notch 334 may be formed between the first long side and the second long side when the stent is deformed to provide for a stronger weld, as shown in FIG. 31. In addition, as shown in FIG. 31 a gap 335 may be provided between the engagement points and the external surface of the mandrel 309 during the deforming step. This gap 335 provides a greater area for weld material, thus, strengthening the weld and reducing heat dissipation through the mandrel during welding, thus, reducing the amount of energy that must be put into the weld.

Additional weld fill material 336 may be provided on the side of each of the engagement points substantially opposite the bridge, as shown in Figs. 33 and 34. The weld fill material 336 is sized and disposed so as to permit the additional weld fill material to be drawn into the weld point during welding.

After the stent has been deformed and the engagement

5 points have contacted each other, the bridge is cut using the
laser. The first side and long sides are then connected using
the laser to form a weld that is preferably wider than the
other portions of the stent. In an especially preferred
embodiment, the weld is about 20% wider than the other
10 portions of the stent and has a width of about 140 microns.
The weld is preferably run from outside-to-in. A plurality of
welding runs is preferably used and in an especially preferred
embodiment two weld-runs are utilized. The weld-run may be
offset from the point where the engagement points contact each
15 other and in a preferred embodiment is offset about .01 mm
from the point where the engagement points contact each other.

The weld may be a spot weld, a plurality of spot welds,
and in a preferred embodiment, the weld comprises 5 spot
20 welds.

In a preferred embodiment, the pattern is cut into the
sheet using multiple-up-etching and comprises the step of
inspecting both sides of the sheet after etching and before
the sheet is disposed on the base. In an especially preferred
25 embodiment the inspection step is carried out using an
automated optical inspection apparatus.

In an especially preferred embodiment, the stent patterns
are adapted so that upon the expansion of the stent against
the internal wall of a vessel substantially no portion of the
30 stent projects into the longitudinal lumen of the stent. The
stent may be finished by electropolishing.

FIGS. 37 to 40 show another embodiment of an apparatus

5 for fabricating a stent constructed in accordance with the invention.

10 A base 401 is provided with a sheet receiving area 402 and is adapted to receive a flat sheet of metal to be formed into a stent. The sheet receiving area 402 is also provided with a mandrel receiving groove 409. In a preferred embodiment, the flat piece of metal has a longitudinal axis, a first major surface, a second major surface, a first long side, and a second long side, with the first and the second long sides substantially parallel to the longitudinal axis.

15 An arm 403 having a first end 404 and a second end 405 is provided.

The first end 404 of the arm is adapted to selectively retain a mandrel 406 having a substantially cylindrical external surface. The second end of the arm 405 is hingedly

20 connected to the base 401 and is adapted for movement in a first direction toward the base 401 and in a second direction away from the base 401 to secure the mandrel 406 against a major surface of the flat sheet of metal. The mandrel 406 is sized to have a cross-sectional diameter substantially equal

25 to or less than the internal cross-sectional diameter of the stent to be fabricated.

A means 407 is provided for deforming the flat piece of metal against and around the external surface of the mandrel so that the flat sheet of metal is deformed into a

30 substantially tubular shape conforming to the external surface of the mandrel with the first long side and the second long side substantially parallel to each other. FIG. 39 shows a

5 top view of one embodiment wherein the means 407 for deforming is a member provided with a deforming tip 408 having a length substantially equal to the length of the first and second long sides of the sheet metal. In a preferred embodiment, the deforming tip is concave, as shown in FIG. 40.

10 In operation, a sheet is placed on the sheet receiving area 402. A mandrel 406 is disposed in the first end 404 of the arm 403 and the arm 403 is moved in the first direction so that the mandrel is in contact with the sheet. The deforming means is then used to deform the sheet around the mandrel a
15 previously discussed. The arm 403 is then moved in the second direction and the mandrel 406 with the sheet wrapped around it is removed from the first end 404 of the arm 403. The first and second long sides are then connected as previously discussed to form the stent. In a preferred embodiment, the
20 mandrel with the sheet wrapped around it is transferred to the stent aligning and welding jig shown in FIGS. 41 to 45.

The stent aligning and welding jig shown in FIGS. 41 to 45 comprises a base 500 having a first end and a second end provided with a first wall 501 having a first end and a second
25 end and a first major surface 502 and a second major surface 503 and a second wall 504 having a first end and a second end and a first major surface 505 and a second major surface 506. The second major surface 503 of the first wall 501 and the first major surface 505 of the second wall 504 define a
30 longitudinal U-shaped channel 507 having a longitudinal axis in the base 500. The first wall 501 is provided with a plurality of slots 508 defining a plurality of first clamping

5 portions 509 having a top end 511 and a bottom end 512 and a
first major surface 502 and a second major surface 503. Each
of the first clamping portions 509 is provided with a first
concave channel 510 disposed at the top end 511 of the second
major surface 503 of the first clamping portion 509 and a
10 second concave channel 513 disposed at the bottom end 512 of
the second major surface 503 of the first clamping portion
509. The first and the second concave channels 510 and 513
are substantially parallel to the longitudinal axis of the U-
shaped channel 507. The second major surface 503 of each of
15 the plurality of first clamping portions 509 is also provided
with a compensation slit 514 disposed between the first
concave channel 510 and the second concave channel 513 that is
substantially parallel to the longitudinal axis of the U-
shaped channel 507.

20 A plurality of second clamping portions 515 is disposed
in the U-shaped channel 507 between the second major surface
503 of the first wall 501 and the first major surface 505 of
the second wall 504. Each of the second clamping portions 515
is disposed in registry with one of the first clamping
25 portions 509. Each of the second clamping portions 515 has a
top end 516, a bottom end 517, a first major surface 518, a
second major surface 519, a first minor surface disposed at
the top end, a second minor surface disposed at the bottom
end, a third minor surface disposed between the top end and
30 the bottom end, and a fourth minor surface disposed opposite
the third minor surface between the top end 516 and the bottom
end 517. Each of the second clamping portions 515 is provided

5 with a first concave channel 521 disposed at the top end 516
of the first major surface 518 of the second clamping portion
515 and a second concave channel 522 disposed at the bottom
end 517 of the first major surface 518 of the second clamping
portion 515. The first and the second concave channels 521
10 and 522 are substantially parallel to the longitudinal axis of
the U-shaped channel 507.

A biasing means 523 is disposed between the first major
surface 505 of the second wall 504 and the second major
surface 503 of each of the of second clamping portions 509 for
15 biasing the first major surface 518 of each of the second
clamping portions 515 against the second major surface 503 of
each of the first clamping portions 509 which are in registry
with each other.

A first mandrel support lever positioning pin 524
20 projects from the third minor surface 520 and a second mandrel
support lever positioning pin 521 projects from the fourth
minor surface of each of the second clamping portions 515.
The mandrel support lever positioning pins 524 and 521 are
substantially parallel to the longitudinal axis of the U-
25 shaped channel.

A biasing control means 522 selectively controls the
distance between the second major surface 503 of each of the
first clamping portions 509 and the first major surface 518 of
each of the second clamping portions 515.

30 A retaining mandrel 523 is disposed in the second concave
channel 513 of the first wall 501 and the second concave
channel 522 in each of the second clamping portions 515.

5 A mandrel support lever 534, as shown in FIG. 42 supports
the stent during the alignment of the first long side of the
sheet with the second long side of the sheet. The lever 534
is provided with a first mandrel support notch 525 for
supporting the first end of the mandrel and a second mandrel
10 support notch 526 for supporting the second end of the
mandrel. A first mandrel support lever positioning pin
engagement surface 527 engages the first mandrel support lever
positioning pin 524 and a second mandrel support lever
positioning pin engagement surface 528 engages the second
15 mandrel support lever positioning pin 521 when the mandrel
support lever is disposed on the second wall 504.

It will be appreciated that various elastic materials
well known to those skilled in the art as suitable for this
purpose may be utilized, e.g., a spring, however, in an
20 especially preferred embodiment, the elastic material is
rubber.

In a preferred embodiment the biasing control means 522
is a threaded screw disposed in each of the first clamping
portions 509 with each of the screws 522 communicating with
25 the first major surface 502 and the second major surface 503
of each of the first clamping portions 509. The screws 522
are selectively movable in a direction toward and away from
the first major surface 518 of the second clamping portion 515
to selectively move the second clamping portion 515 in a
30 direction toward and away from the first clamping portions 509
to selectively vary the distance between the second major
surface 503 of each of the first clamping portions 509 and the

5 first major surface 518 of each of the second clamping
portions 515.

In operation, the mandrel with the sheet wrapped around
it is secured in the first concave channels 510 and 521. The
biasing control means 522, e.g., a screw, is adjusted to
10 secure the mandrel in the first concave channels while
permitting the first and second long sides of the sheet to be
adjusted so that the contact points are aligned as desired.
In a preferred embodiment, the mandrel support lever shown in
FIG. 42, is utilized to support the mandrel during the
15 alignment operation. As shown in FIG. 45, the first mandrel
support notch supports the first end of the mandrel and the
second mandrel support notch supports the second end of the
mandrel. The first mandrel support lever positioning pin
surface 527 engages the first mandrel support lever
20 positioning pin 524 and the second mandrel support lever
positioning pin surface 528 engages the second mandrel support
positioning pin 521 so as to align the mandrel support lever
534 when it is supporting the mandrel.

FIGS. 46 to 48 show a jig 612 for electropolishing a
25 tubular stent, comprising a rack 600 having a first end 601
and a second end 602 and provided with a plurality of stent
electropolishing mounts 603. Each of the mounts 603 is
provided with a base 604 and an electrically conductive first
member 605 having a first end 606 connected to the base 604
30 and a second end 607 adapted to selectively contact the
external surface of the tubular stent to be electropolished
without damaging its external surface. The mounts 603 are

5 also provided with an electrically non-conductive second member 608 having a first end 609 connected to the base and a second end 610 adapted to be selectively disposed within the longitudinal bore of the stent without damaging the surface defining the longitudinal bore. The first member 605 and the
10 second member 608 are also adapted so as to bias the second end 610 of the second member 608 towards the second end 607 of the first member 605 in an amount sufficient to secure the stent between said first and the second members 605 and 608. The advantage of a mount constructed in accordance with
15 applicants' invention is that the electrically conductive member 605 contacts the external surface of the stent. This reduces the likelihood of undulations and erosion lines occurring on the surface defining the longitudinal bore. These erosion lines frequently occur in stents electropolished
20 utilizing conventional mounts which place the electrically conductive member against the surface defining the longitudinal bore. Electropolishing a stent with Applicants' mount reduces the likelihood that the longitudinal lumen of the stent will have an irregular surface which could result in
25 turbulent fluid flow which could result in thrombosis or platelet aggregation.

In a preferred electropolishing method a stent is placed on a rack constructed as previously discussed. The method comprises immersing the stent in an electropolishing bath and
30 applying electrical current to the first member for a predetermined period of time; and changing the point where the second end of the first member contacts the external surface

5 of the stent prior to the expiration of the predetermined
period of time. Changing the point of contact minimizes the
concentration of undulations or erosion lines at any given
point on the stent near the point of contact of the
electrically conductive member. The point of contact may be
10 changed by rotating the stent. In an especially preferred
embodiment, the point of contact is changed by varying the
distance between the stent and the base by longitudinally
moving the stent toward or away from the base 604 as shown in
FIGS. 46 and 47. The point of contact is changed at about the
15 midpoint of the predetermined period of time. In an
especially preferred embodiment, the treatment is interrupted
before the expiration of the predetermined time, the effect of
the electropolishing prior to the interruption step is
evaluated, and the remaining period of the predetermined time
20 is adjusted to compensate for any variations in the amount of
material actually removed prior to the interruption step. The
treatment may be interrupted at any time, however,
interruption at about the midpoint of the predetermined period
of time is preferred.

25 Pieces of sacrificial material 611 may be added at the
first end 601 and the second end 602 of the rack 600 to
compensate for the additional material normally removed from
stents disposed at the first end and the second end of the
rack as shown in FIG 48. The material is selected and added
30 in an amount sufficient to substantially equalize the amount
of additional material normally removed from the stents
disposed first and second ends of the rack.

5 In yet another preferred method of electropolishing a
stent, the stent is manufactured as previously discussed
however, when deforming the pattern into a tubular shape so
that the first long side pairs of engagement points contact
the second long side pairs of engagement points, a portion of
10 the stent is allowed to remain attached to the sheet of metal,
as shown in FIGS. 49 and 50 (which is an end view taken along
line A-A of FIG. 49). The bridge is then cut, the engagement
points are connected to form the stent, the stent is
electropolished by connecting an electrode to the sheet, and
15 the stent is then removed from the sheet. This reduces the
likelihood of damage to the stent because the sheet to which
the stent is attached is disposable. This method also
provides an additional advantage because the disposable sheet
to which the stent is attached acts as sacrificial material as
20 previously discussed.

 It will be appreciated by persons skilled in the art
that the present invention is not limited to what has been
particularly shown and described hereinabove. Rather the
scope of the present invention is defined only by the claims
25 which follow.

What is claimed is:

1. A stent aligning and welding jig comprising:
 - a) a base having a first end and a second end, a first wall having a first end and a second end and a first major surface and a second major surface; a second wall having a first end and a second end and a first major surface and a second major surface, said second major surface of said first wall and said first major surface of said second wall defining a longitudinal U-shaped channel having a longitudinal axis in said base, said first wall provided with a plurality of slots defining a plurality of first clamping portions having a top end and a bottom end and a first major surface and a second major surface, each of said first clamping portions provided with a first concave channel disposed at said top end of said second major surface of said first clamping portion and a second concave channel disposed at said bottom end of said second major surface of said first clamping portion, said first and said second concave channels substantially parallel to said longitudinal axis of said U-shaped channel; said first wall of each of said plurality of first clamping portions provided with a compensation slit disposed between said first concave channel and said second concave channel, said compensation slit substantially parallel to said longitudinal axis of said U-shaped channel;
 - b) a plurality of second clamping portions disposed in said U-shaped channel between said second major surface of said first wall and said first major surface of said second wall, each of said second clamping portions disposed in registry with one of said first clamping portions, each of said second clamping portions having a top end, a bottom

end, a first major surface, a second major surface, a first minor surface disposed at said top end, a second minor surface disposed at said bottom end, a third minor surface disposed between said top end and said bottom end, and a fourth minor surface disposed opposite said third minor surface between said top end and said bottom end, each of said second clamping portions provided with a first concave channel disposed at said top end of said first major surface of said second clamping portion and a second concave channel disposed at said bottom end of said first major surface of said second clamping portion, said first and said second concave channels substantially parallel to said longitudinal axis of said U-shaped channel;

- c) a biasing means disposed between said first major surface of said second wall and said second major surface of each of said plurality of second clamping portions for biasing said first major surface of each of said second clamping portions against said second major surface of each of said first clamping portions which are in registry with each other;
- d) a first mandrel support lever positioning pin projecting from said third minor surface and a second mandrel support lever positioning pin projecting from said fourth minor surface of each of said second clamping portions, said mandrel support lever positioning pins substantially parallel to said longitudinal axis of said U-shaped channel;
- e) a biasing control means for selectively controlling the distance between said second major surface of each of said first clamping portions and said first major surface of each of said second clamping portions;

- f) a retaining mandrel disposed in said second concave channel of said first wall and said second concave channel in each of said second clamping portions; and
- g) a mandrel support lever for supporting said stent during the alignment of said first long side of said sheet with said second long side of said sheet, said lever provided with a first mandrel support notch for supporting said first end of said mandrel, a second mandrel support notch for supporting said second end of said mandrel, a first mandrel support lever positioning pin engagement surface for engaging said first mandrel support lever positioning pin and a second mandrel support lever positioning pin engagement surface for engaging said second mandrel support lever positioning pin when said mandrel support lever is disposed on said second wall.

2. The apparatus of claim 1, wherein said biasing means is an elastic material.

3. The apparatus of claim 2, wherein said elastic material is rubber.

4. The apparatus of claim 2, wherein said elastic material is a spring.

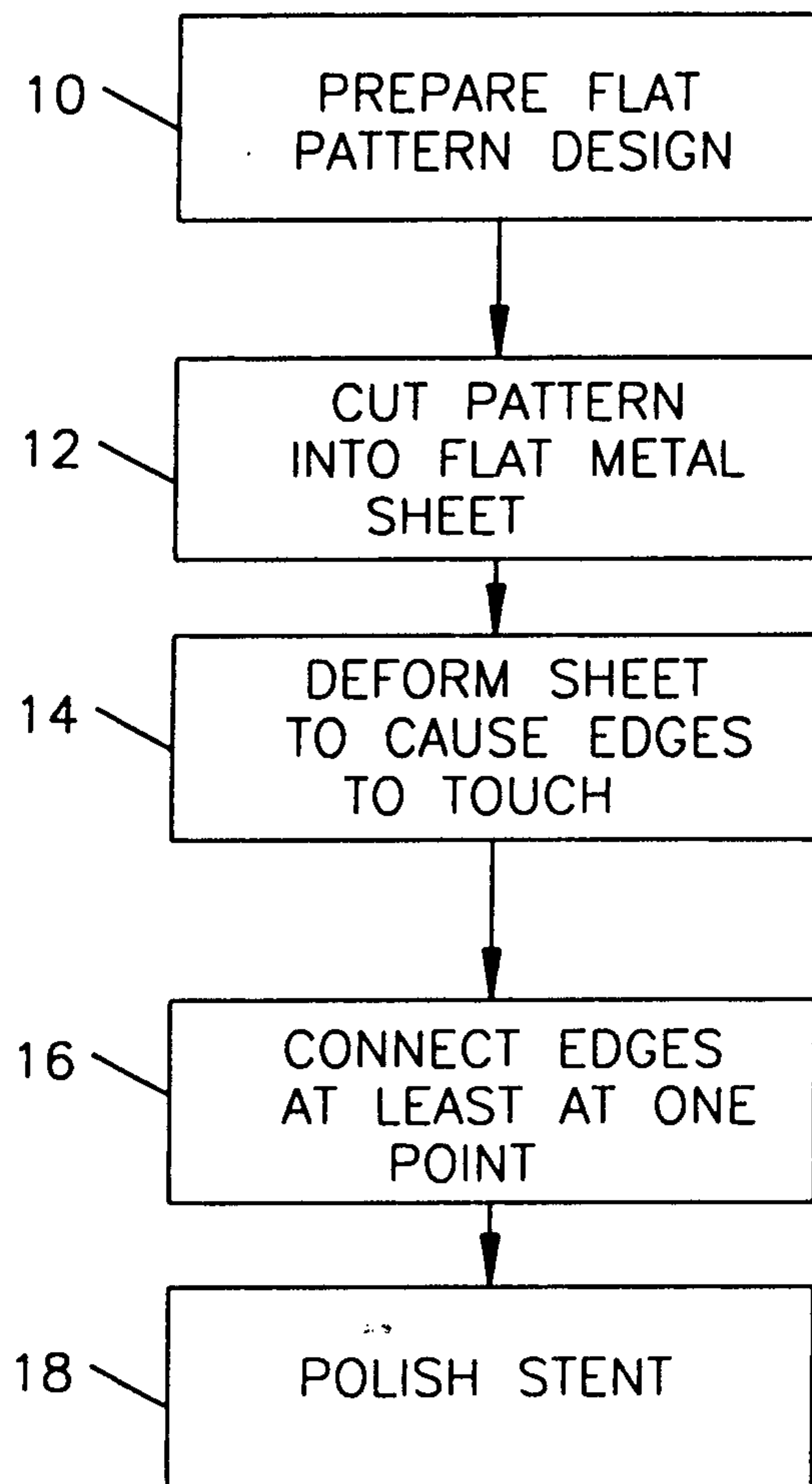
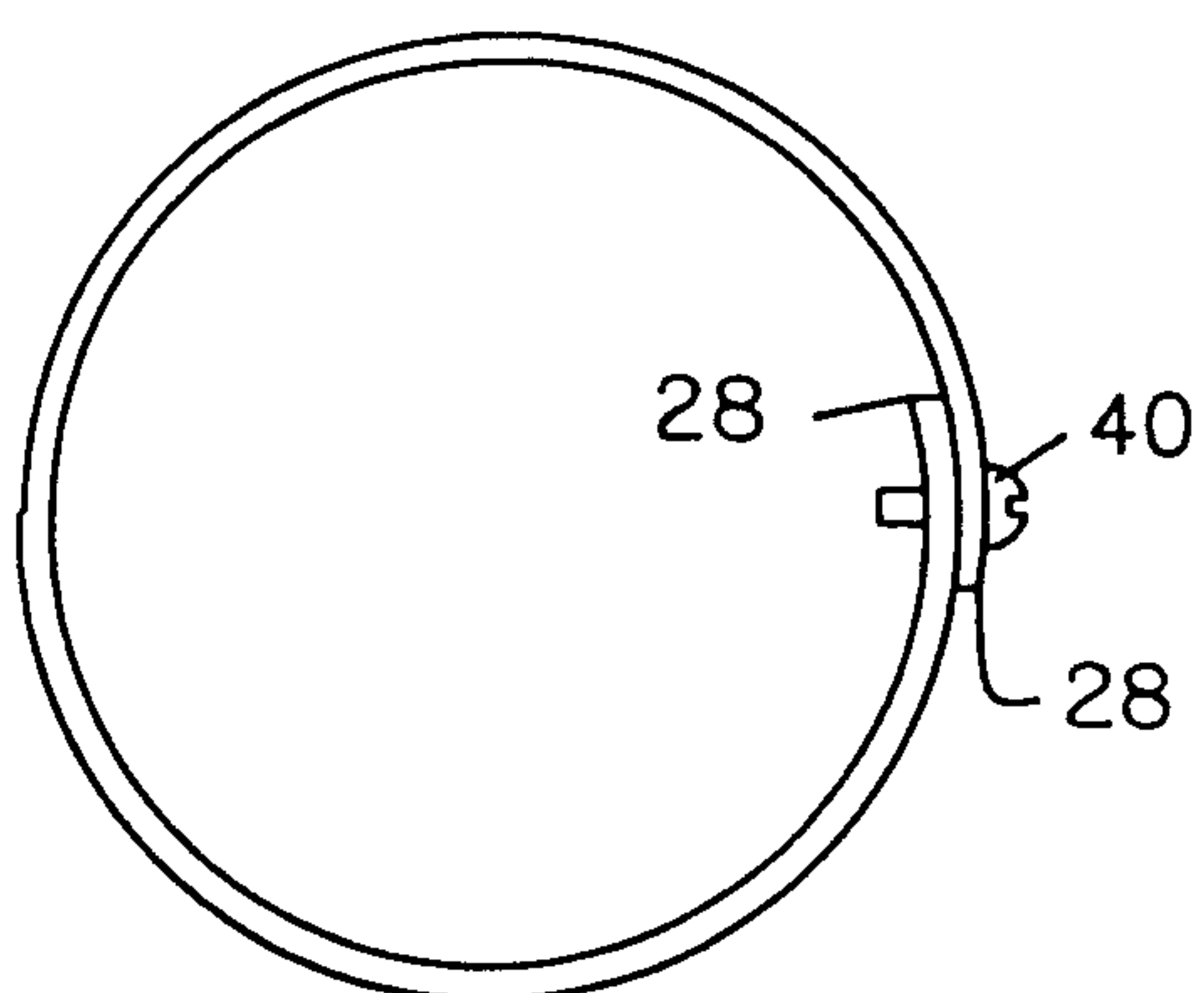
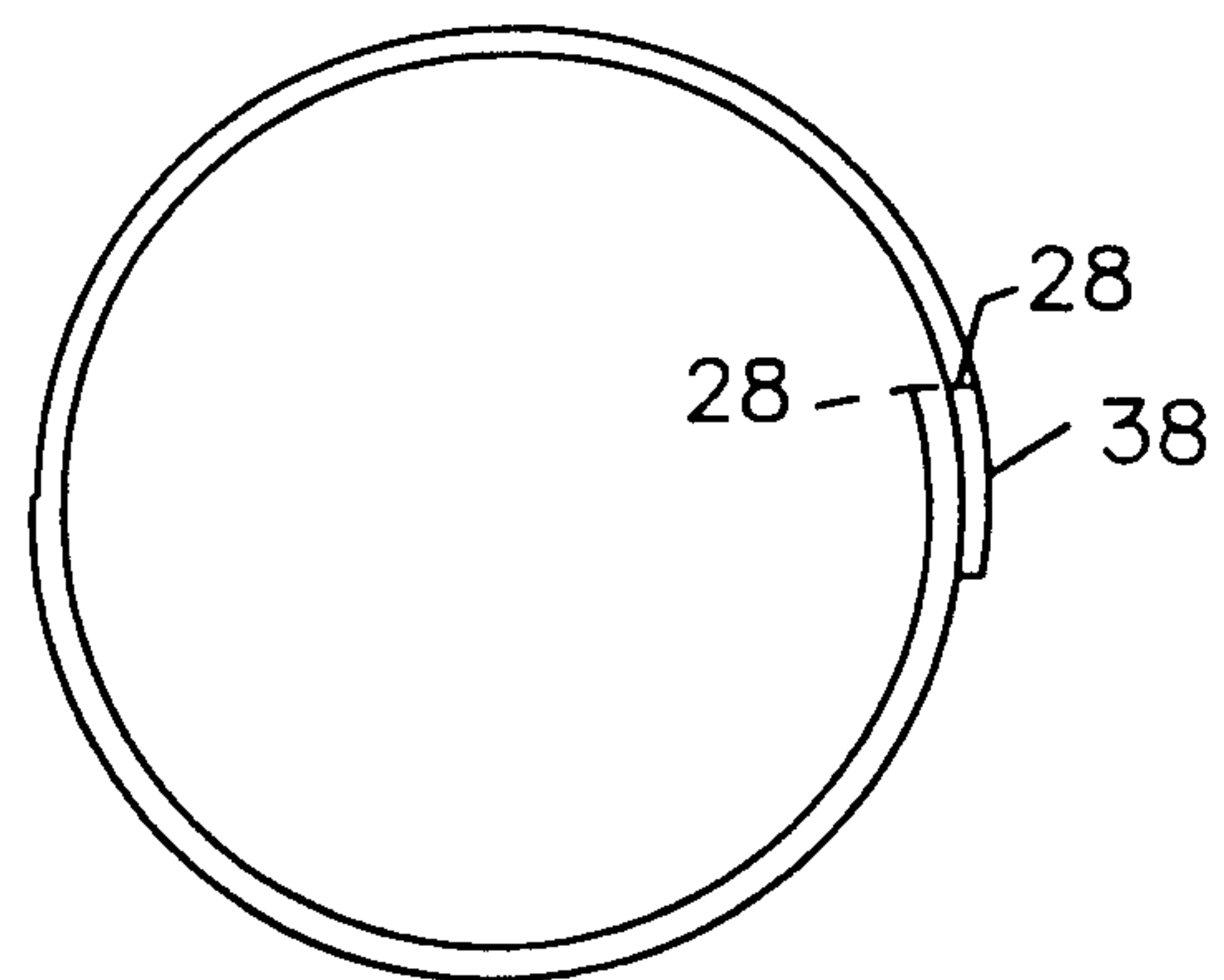
5. The apparatus of claim 1, wherein said biasing control means is a threaded screw disposed in each of said first clamping portions, each of said screws communicating with said first major surface and said second major surface of each of said first clamping portions and selectively movable in a direction toward and away from said first major surface of said second clamping portion to selectively move said second clamping

portion in a direction toward and away from said first clamping portions to selectively vary the distance between said second major surface of each of said first clamping portions and said first major surface of each of said second clamping portions.

6. A jig for electropolishing a tubular stent, comprising:

a rack having a first end and a second end, said rack provided with a plurality of stent electropolishing mounts, each of said mounts having

- a) a base;
- b) an electrically conductive first member having a first end connected to said base and a second end adapted to selectively contact the external surface of said tubular stent without damaging said external surface;
- c) an electrically non-conductive second member having a first end connected to said base and a second end adapted to be selectively disposed within the longitudinal bore of said stent without damaging said longitudinal bore, said first member and said second member further adapted so as to bias said second end of said second member towards said second end of said first member in an amount sufficient to secure said stent between said first and said second members.

**FIG. 1****FIG. 6****FIG. 5A**

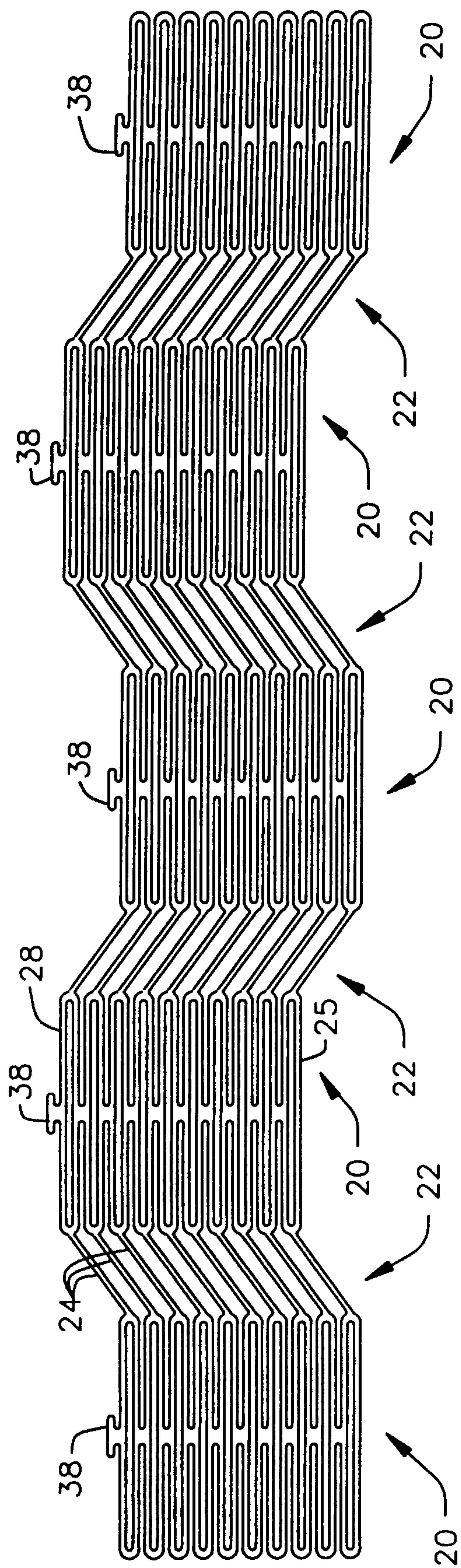
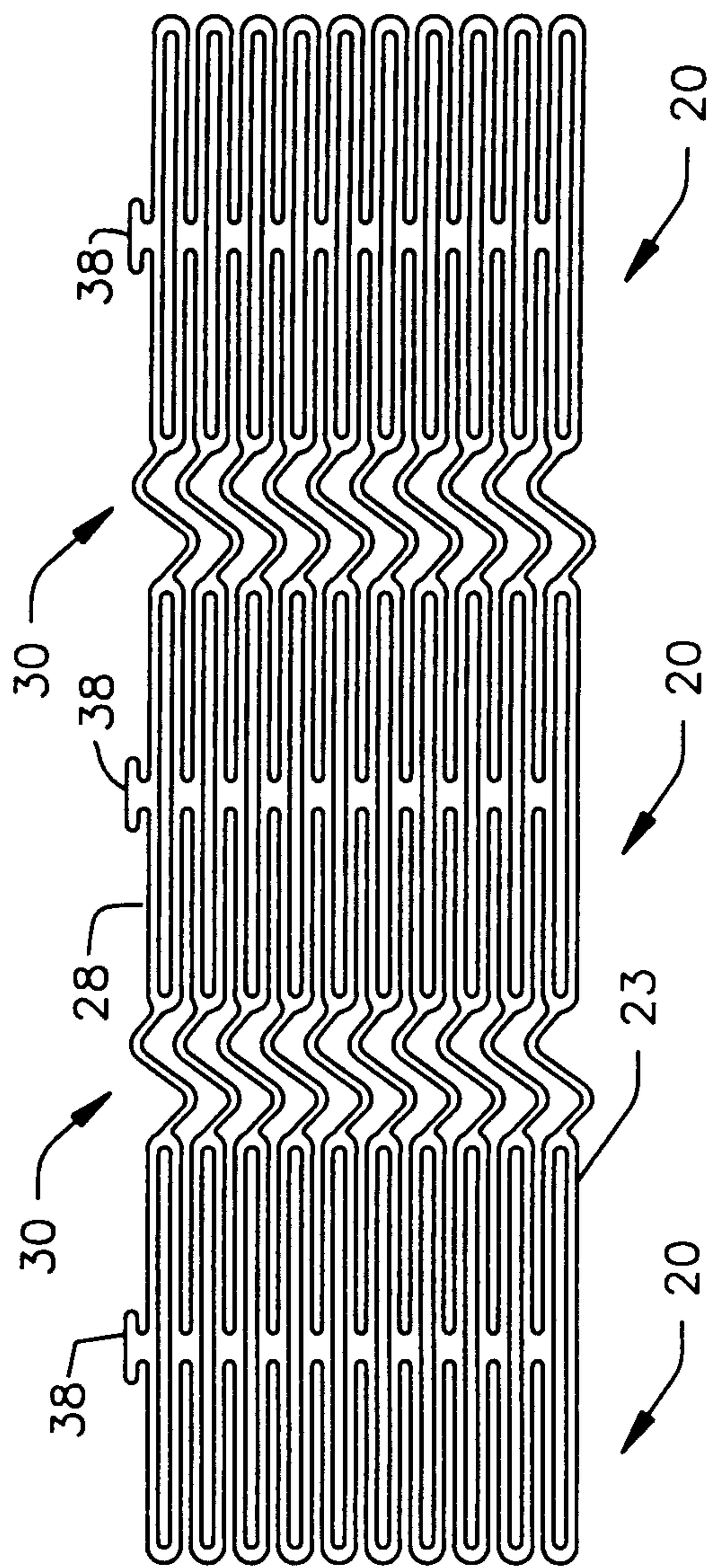
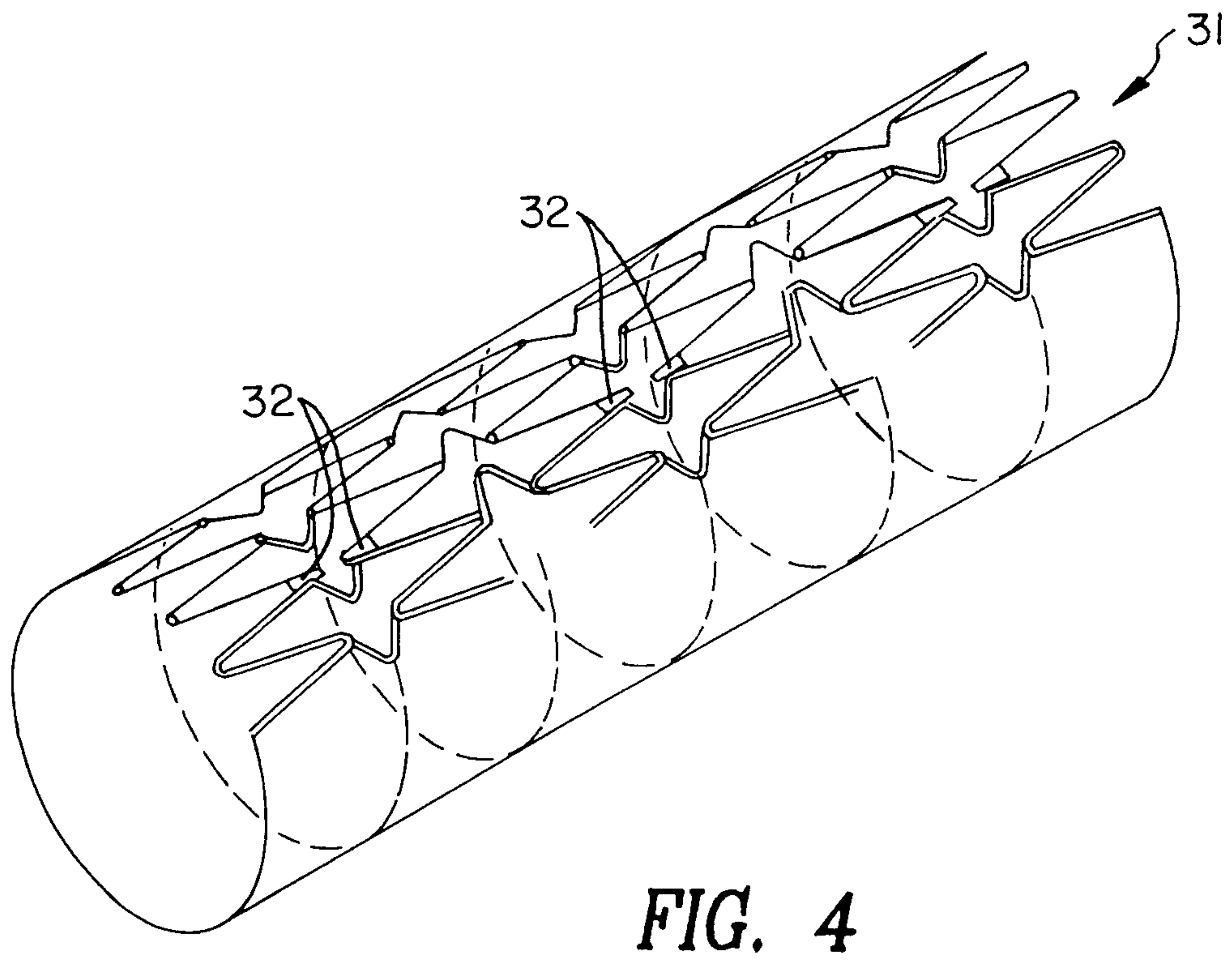
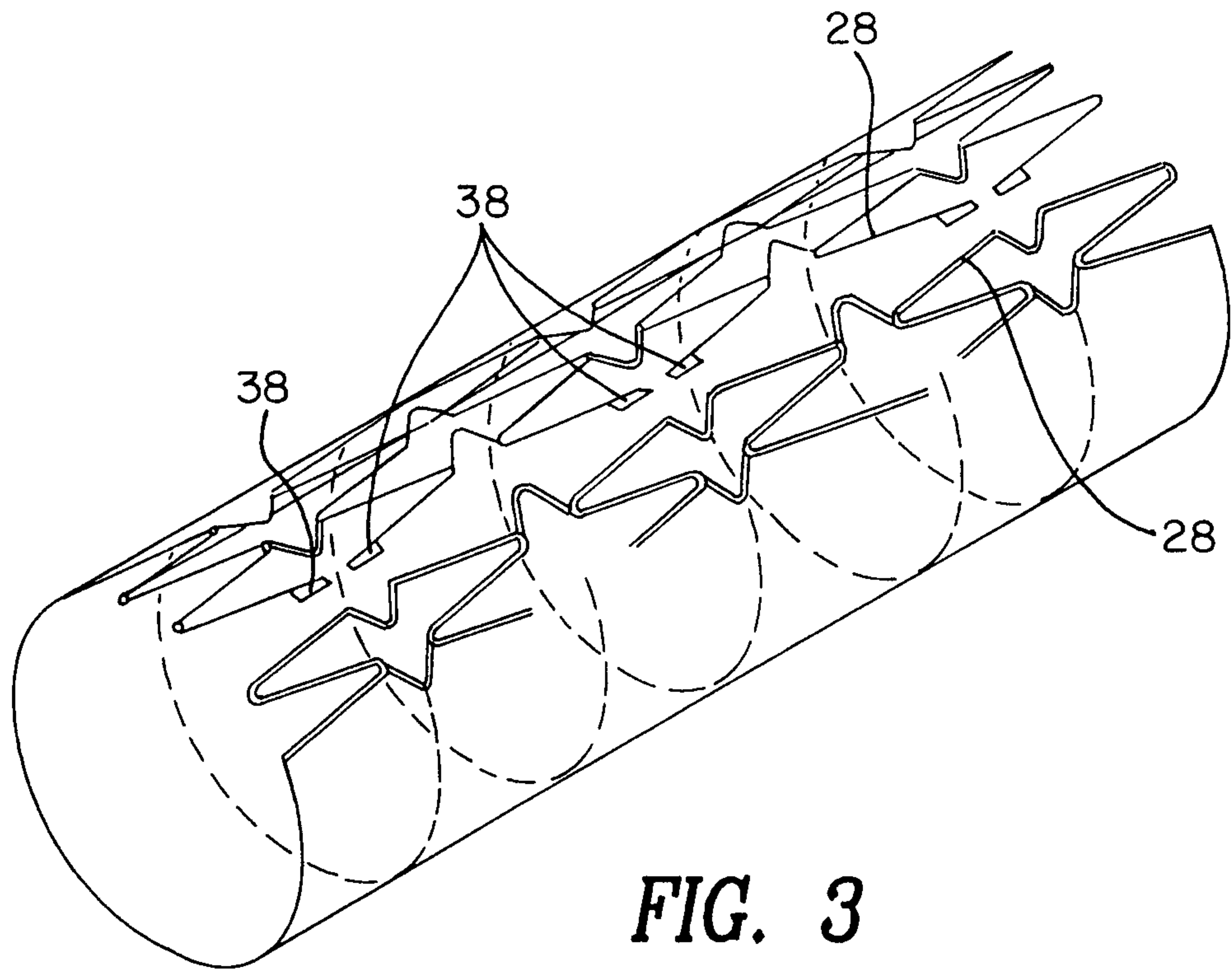


FIG. 2A





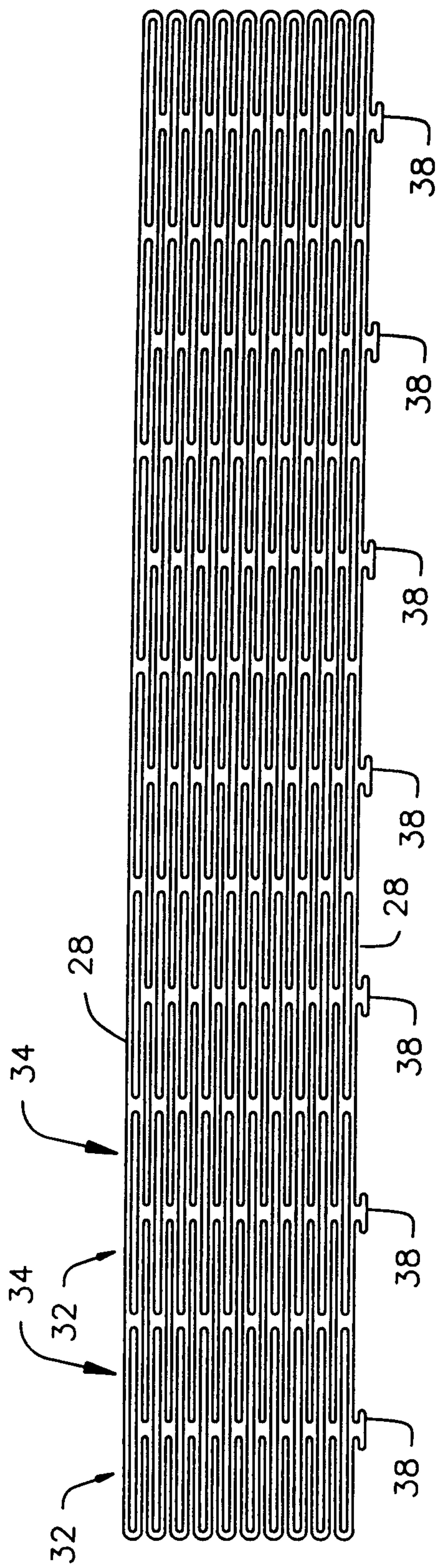


FIG. 2C

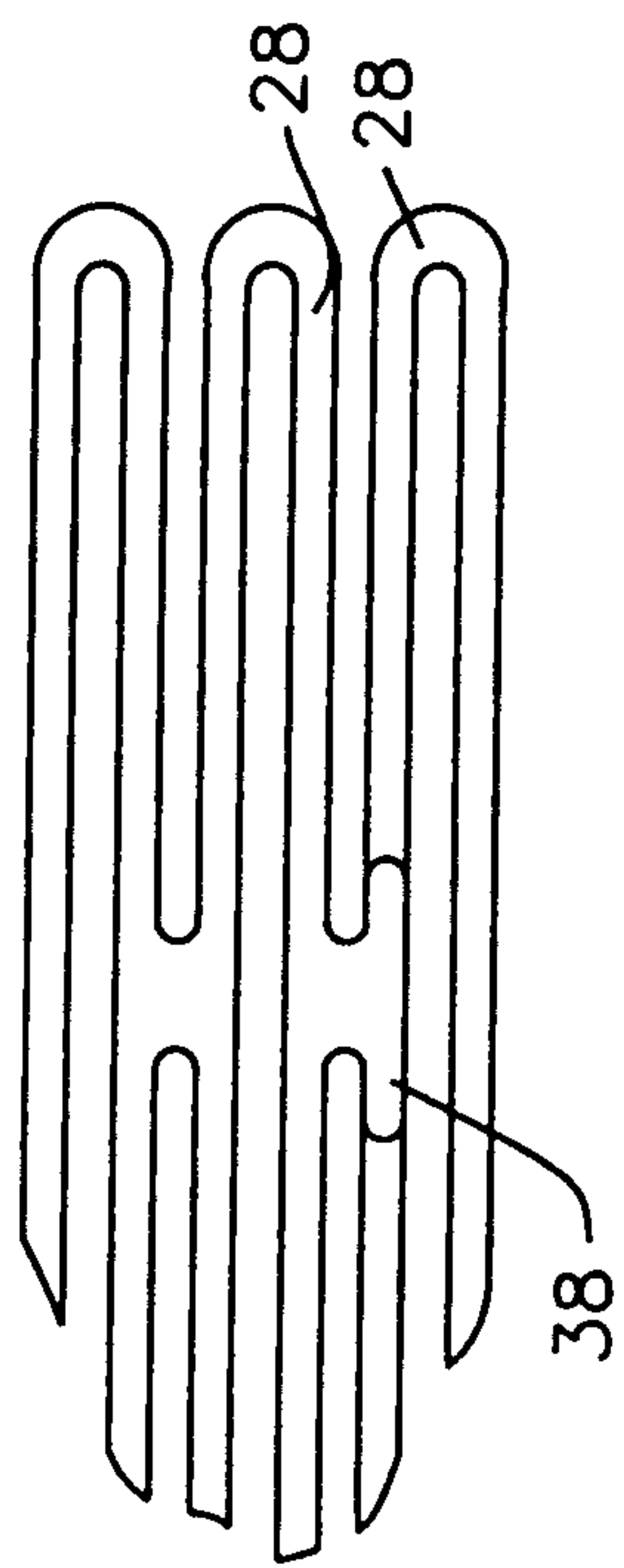


FIG. 5B

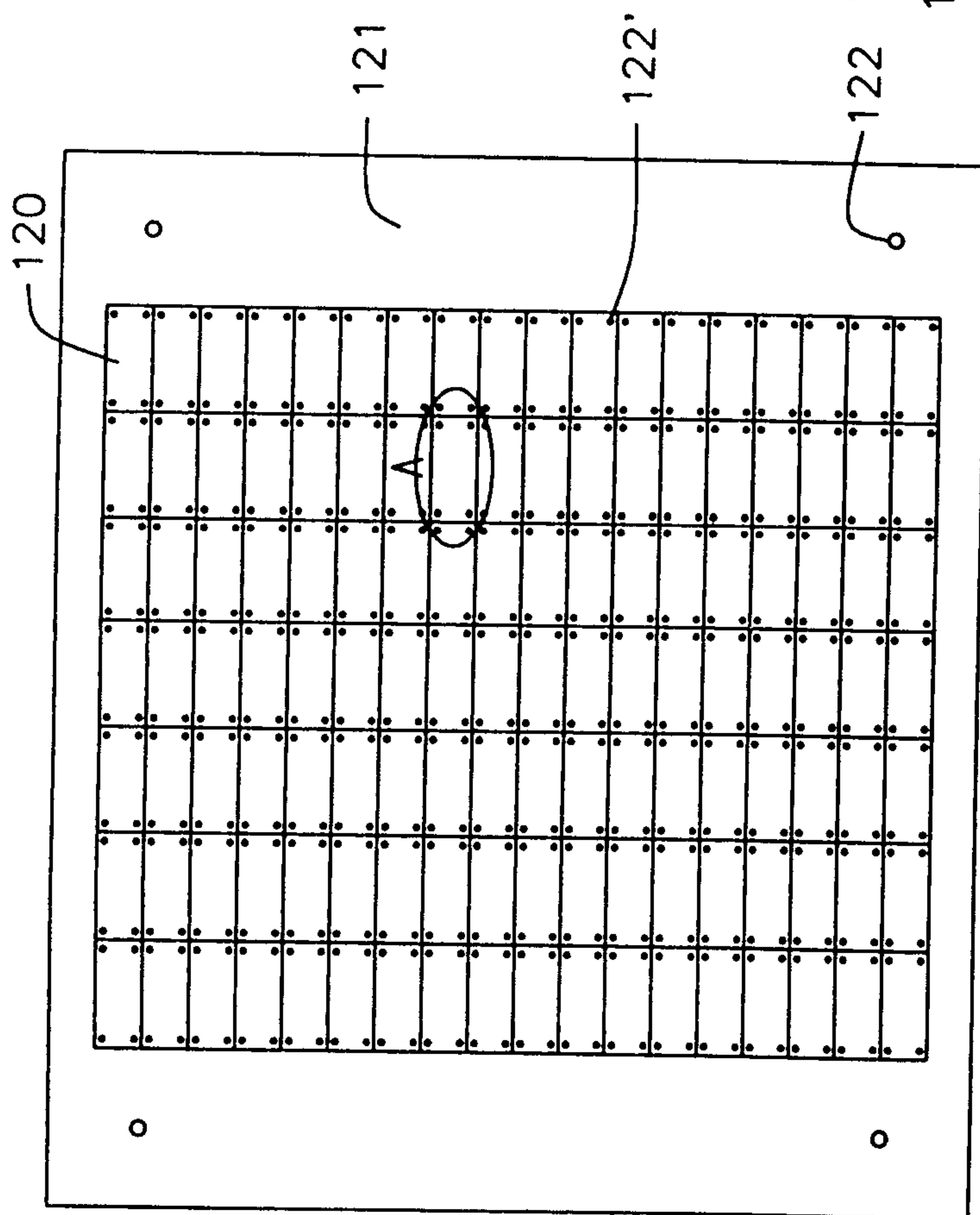


FIG. 7

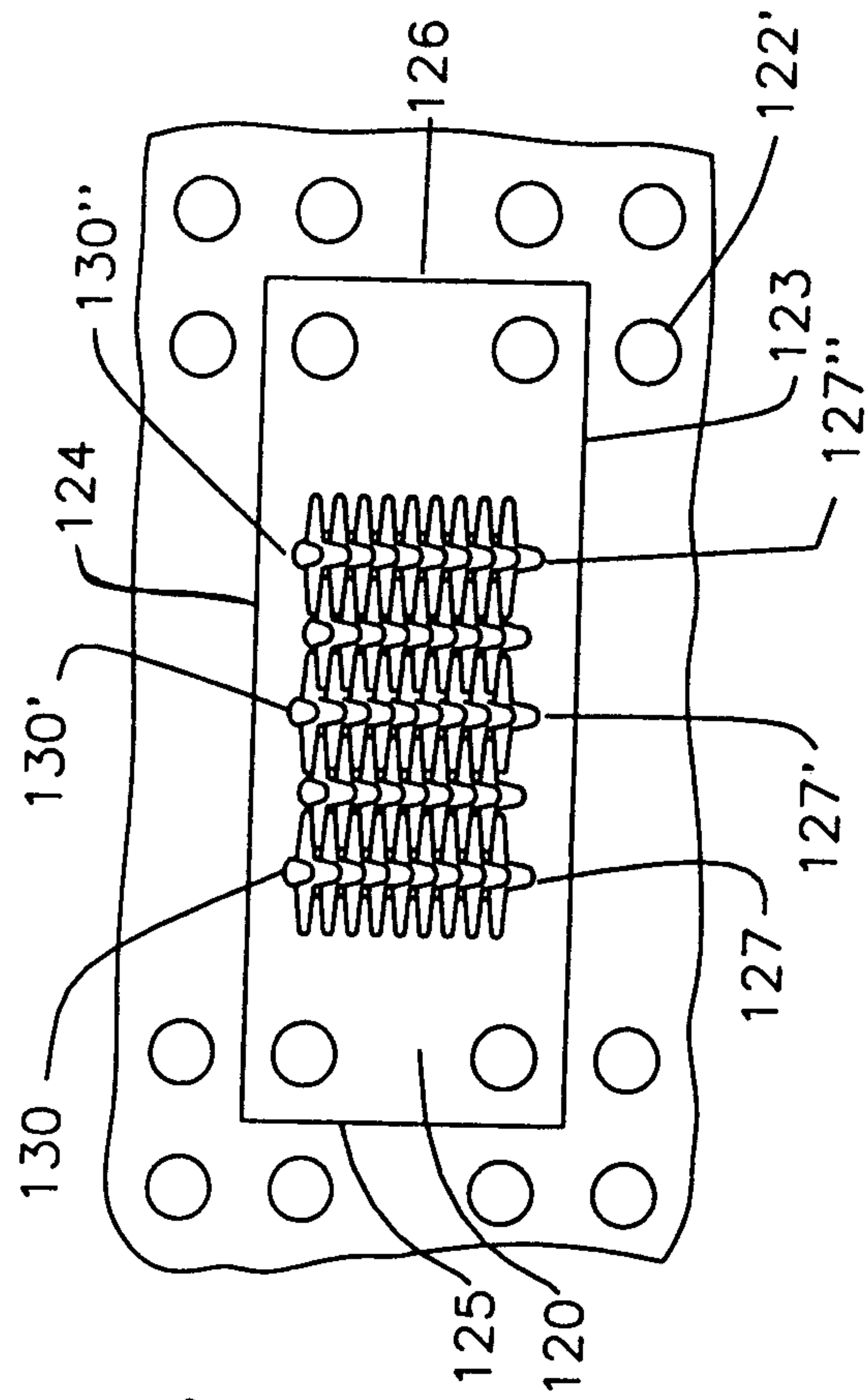


FIG. 8

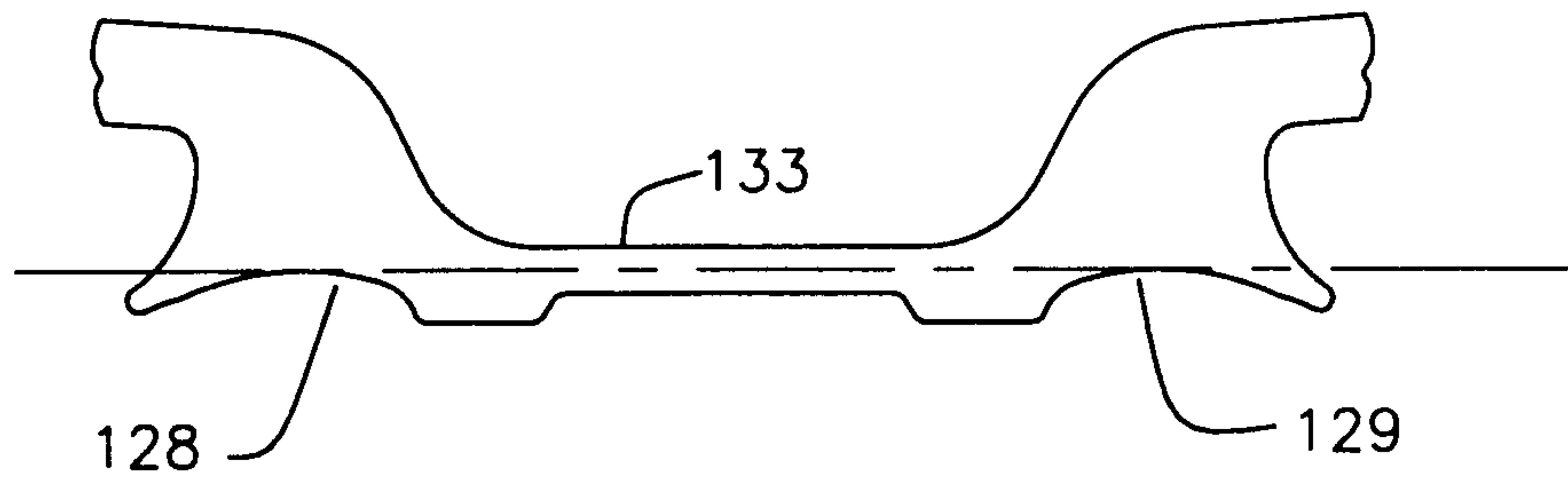


FIG. 9

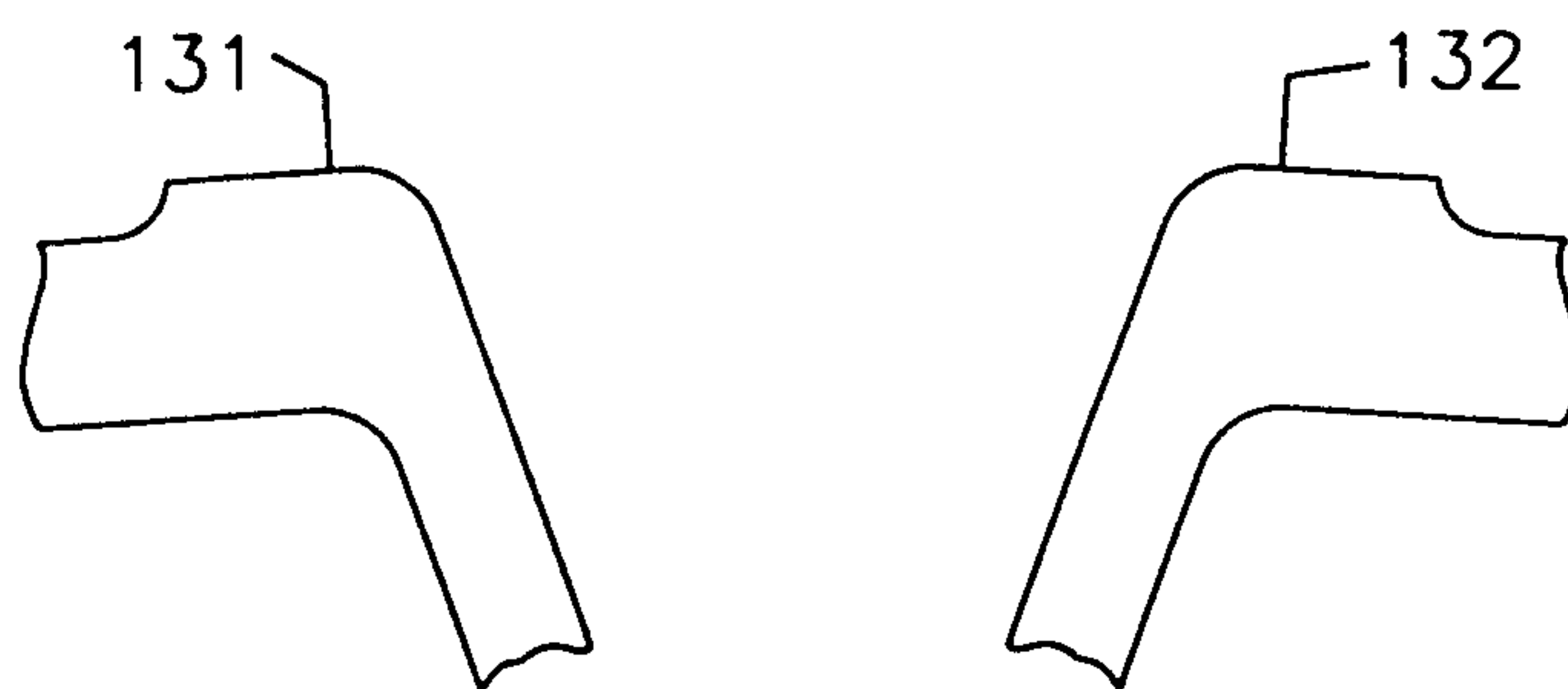


FIG. 10

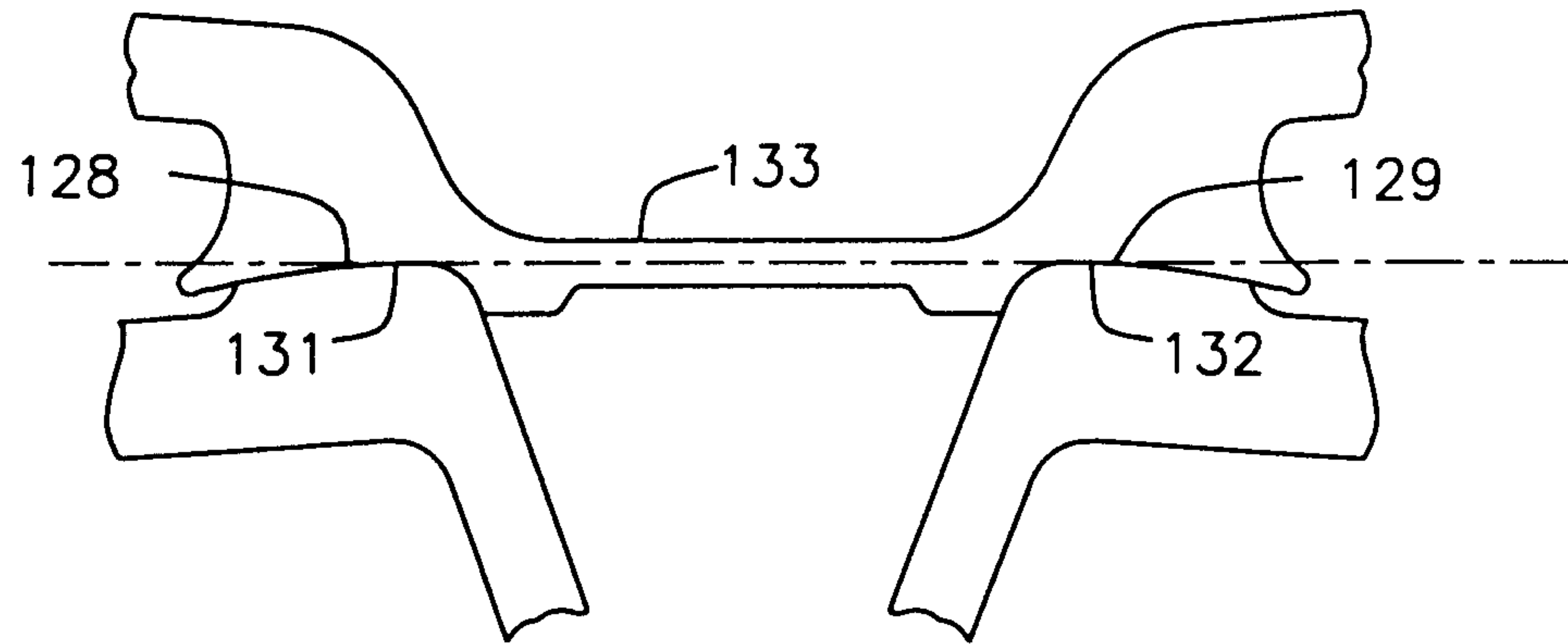


FIG. 11

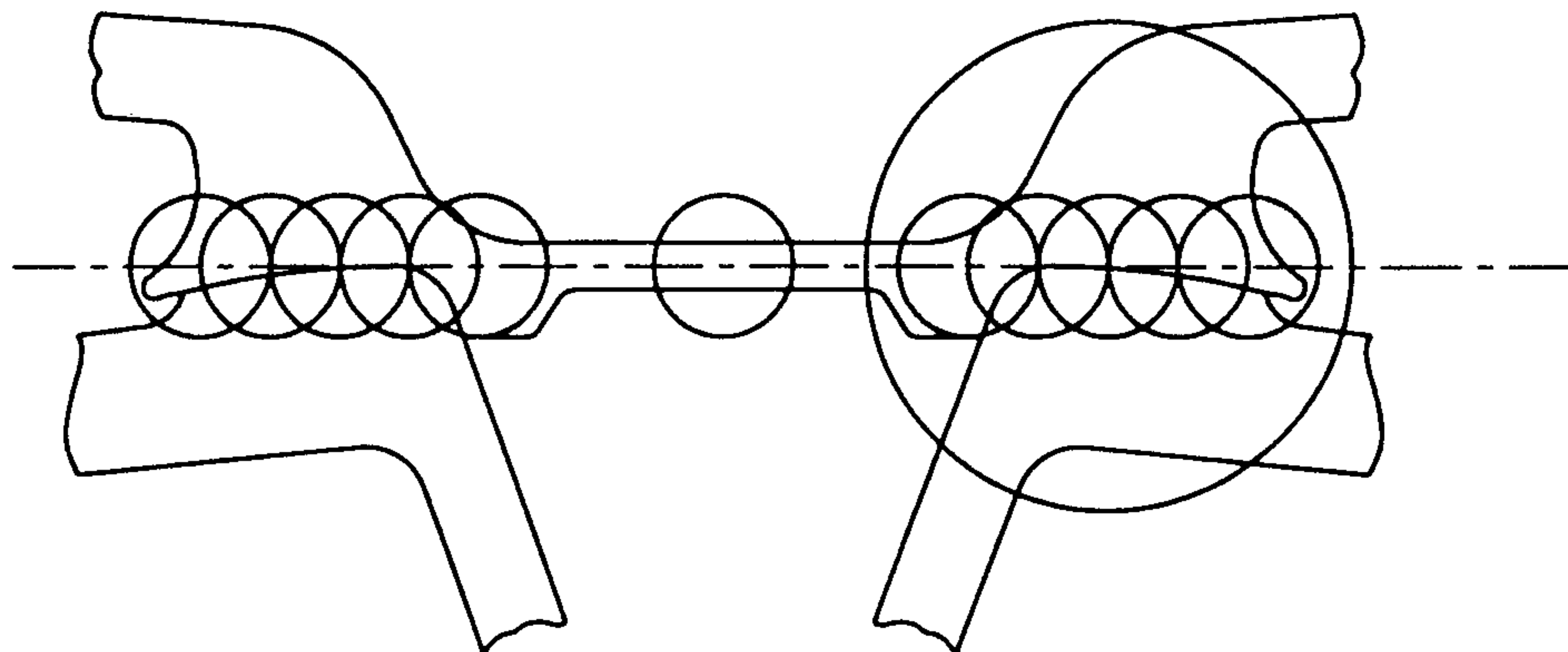


FIG. 12

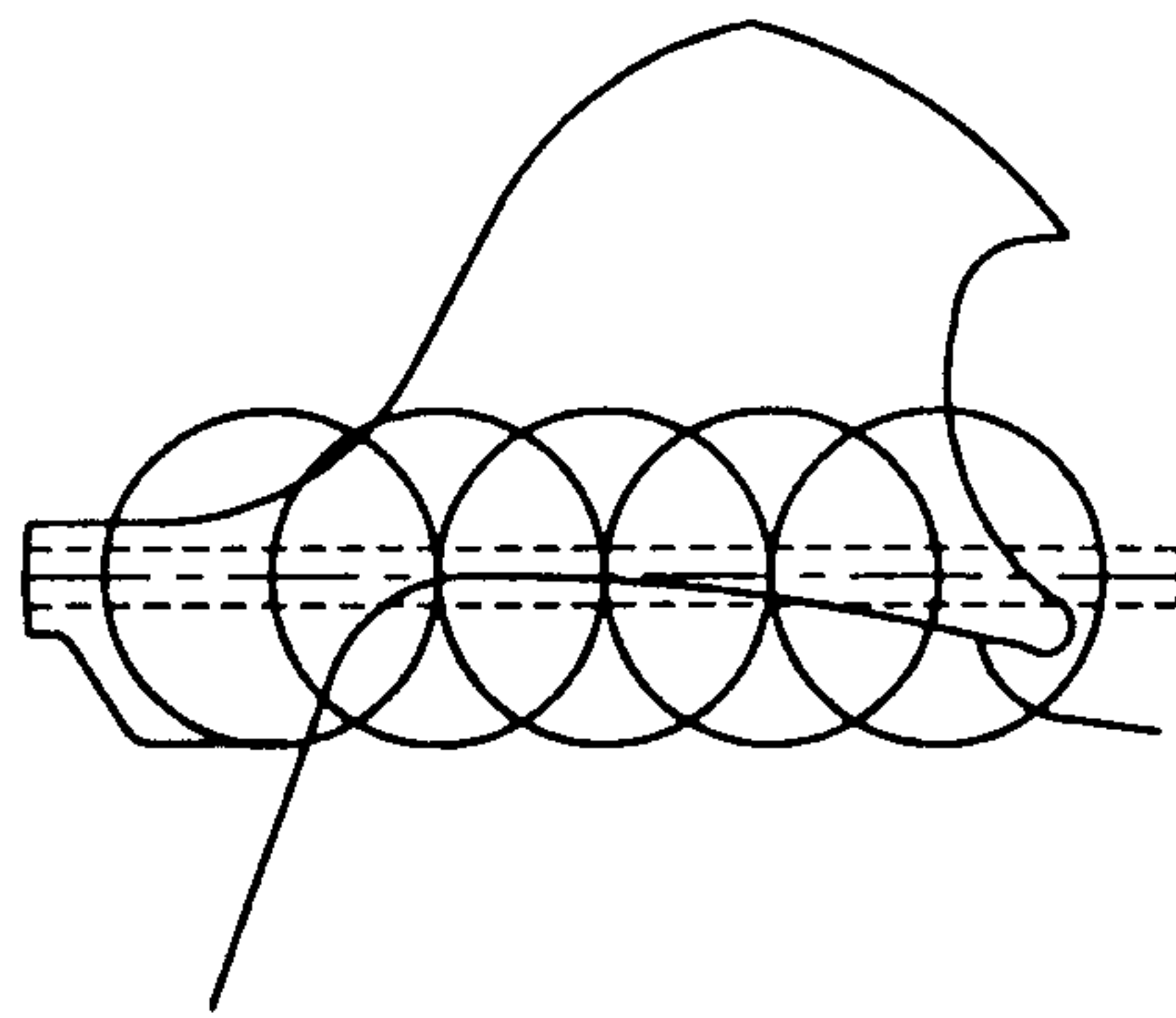


FIG. 13

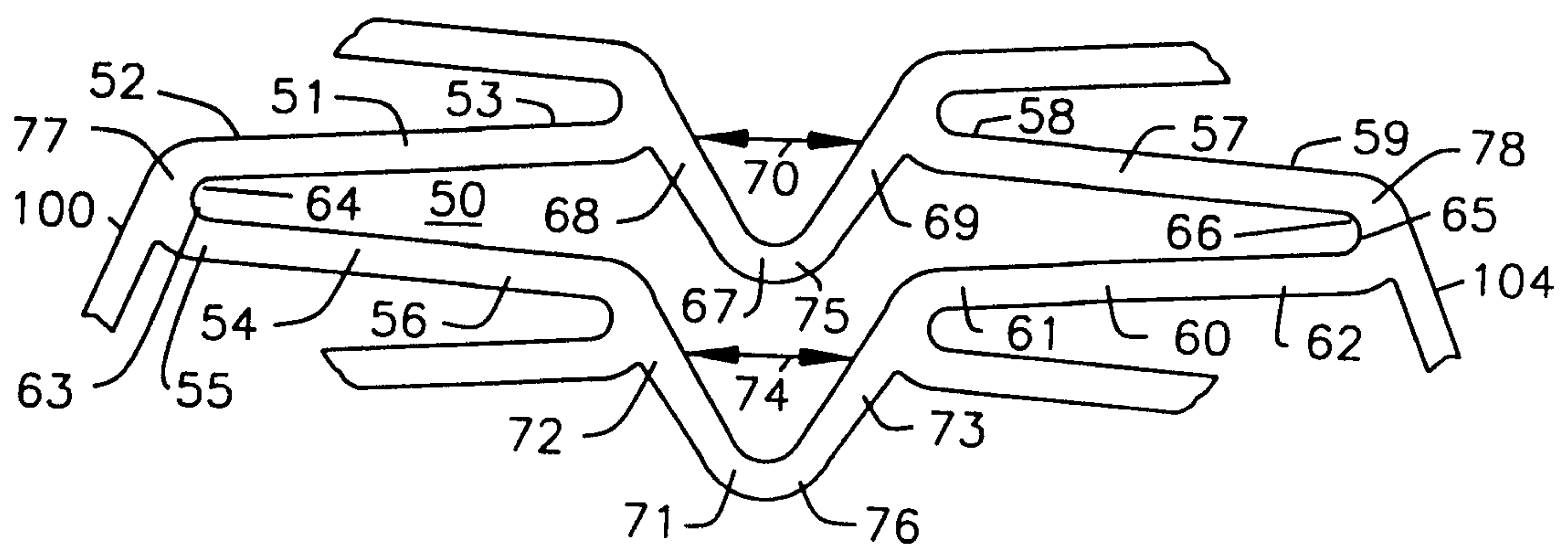


FIG. 14

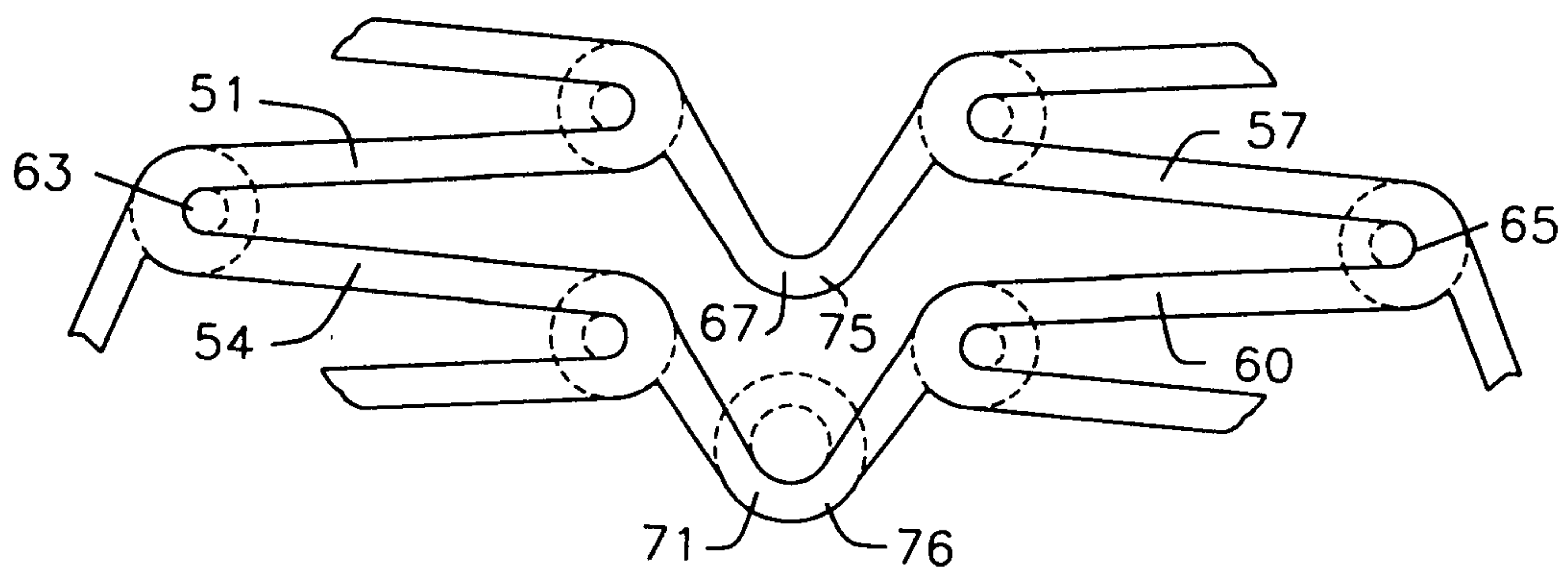


FIG. 15

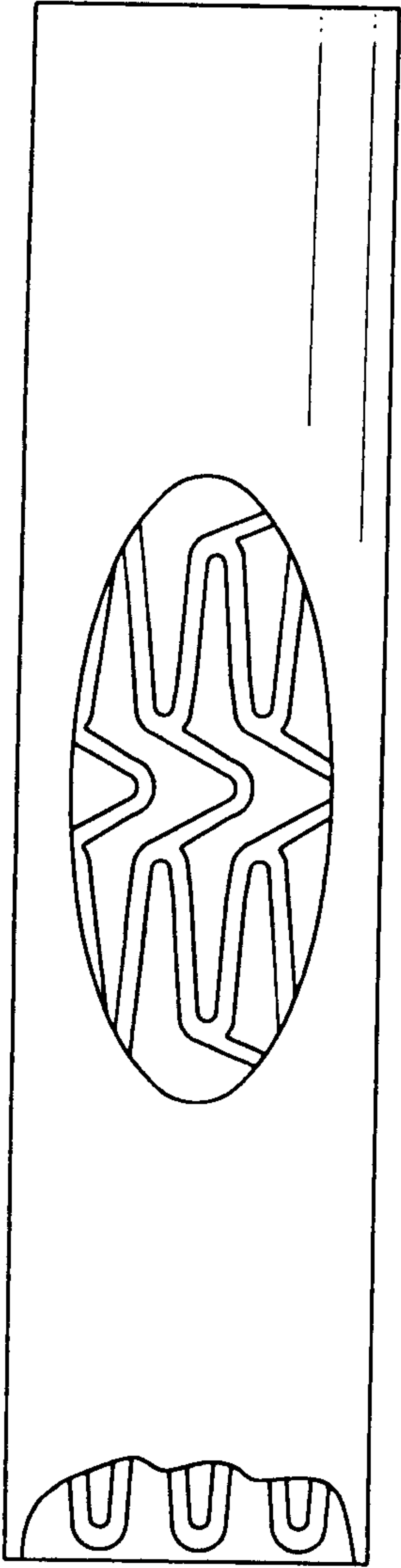


FIG. 16

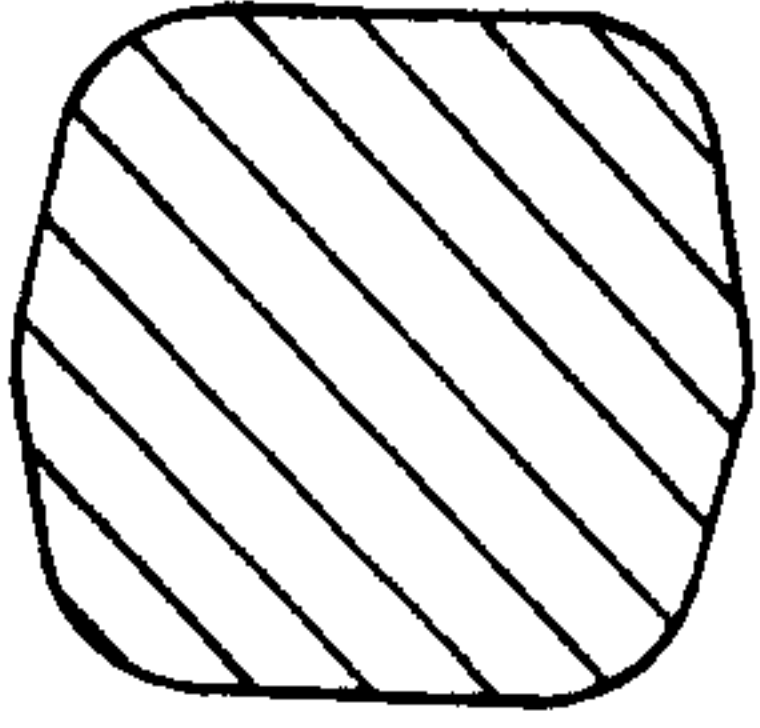


FIG. 18

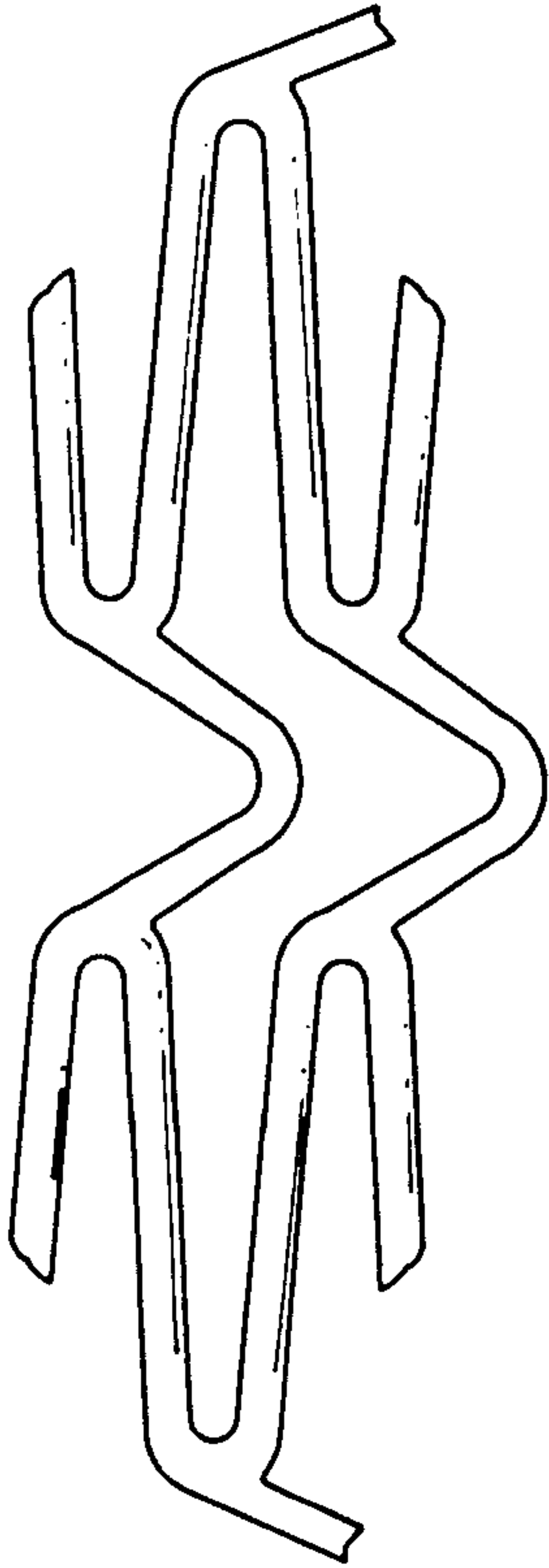


FIG. 17

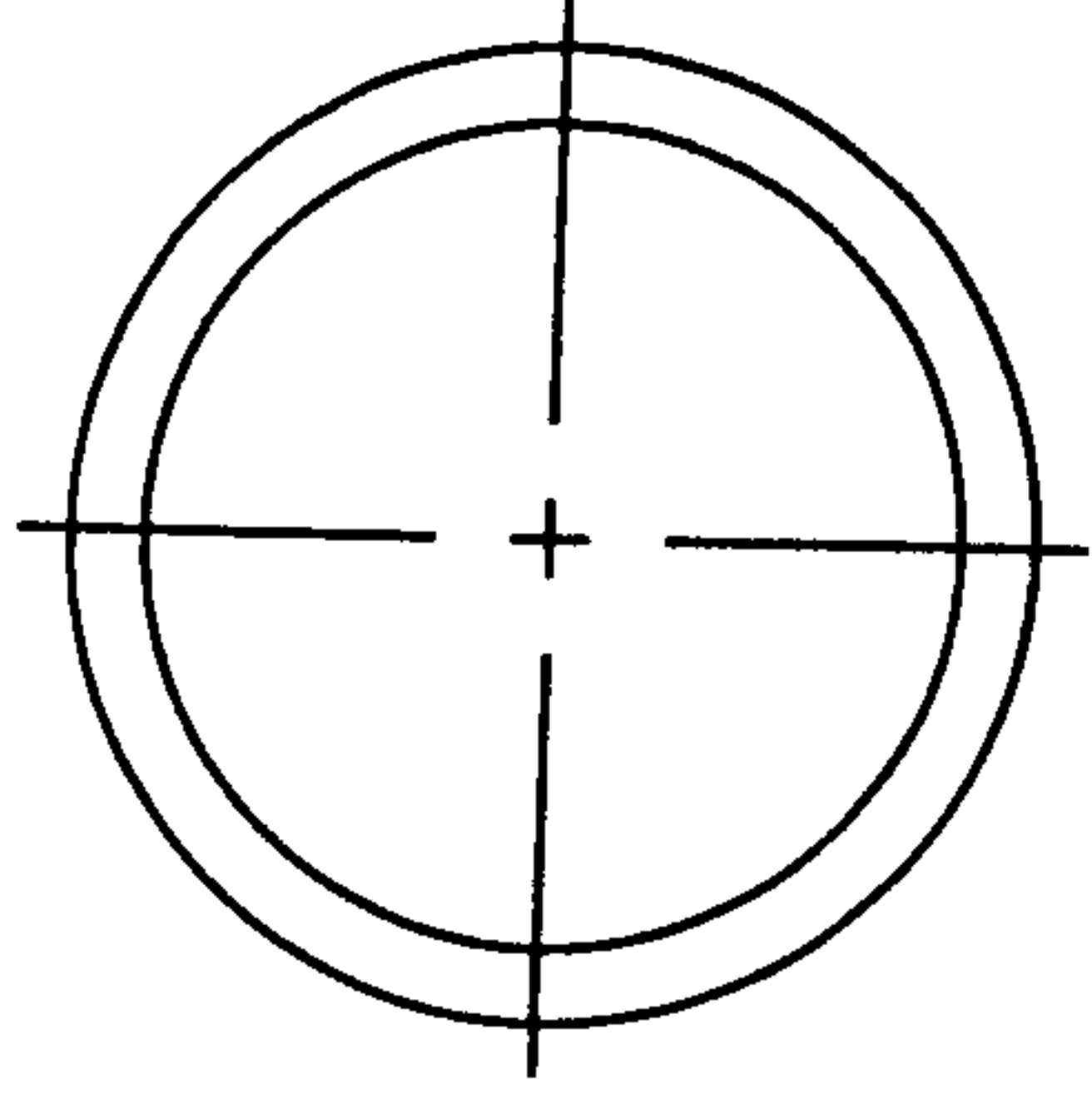


FIG. 19

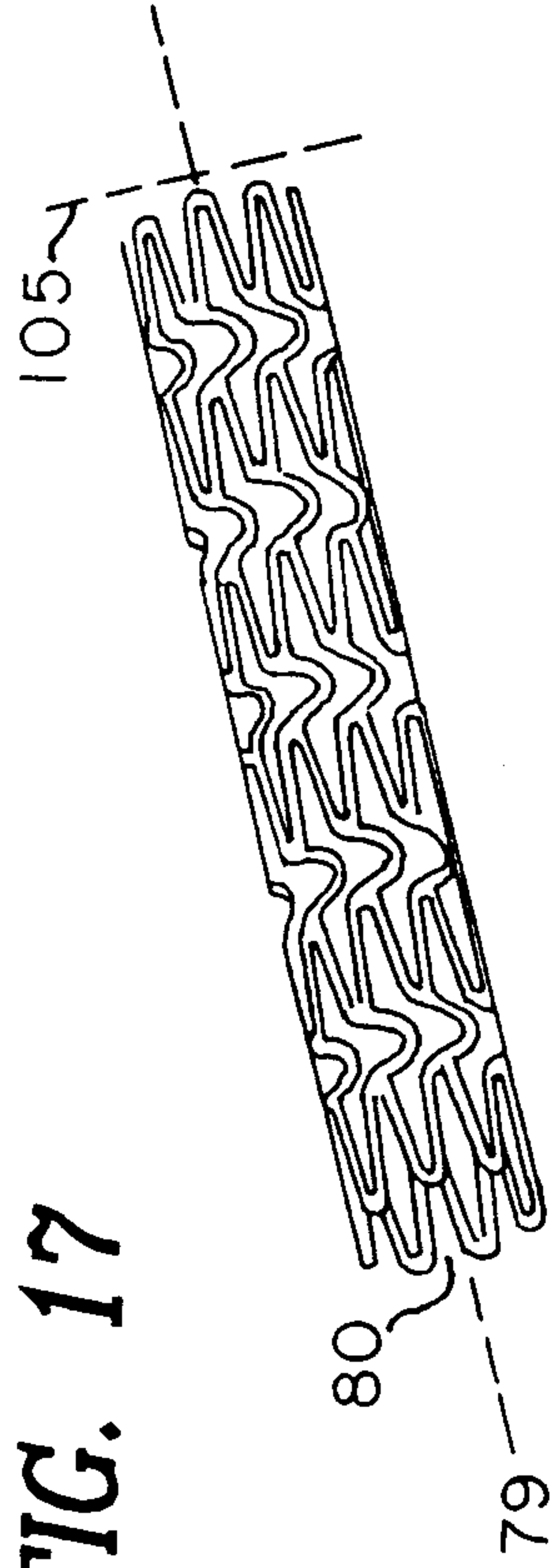


FIG. 20

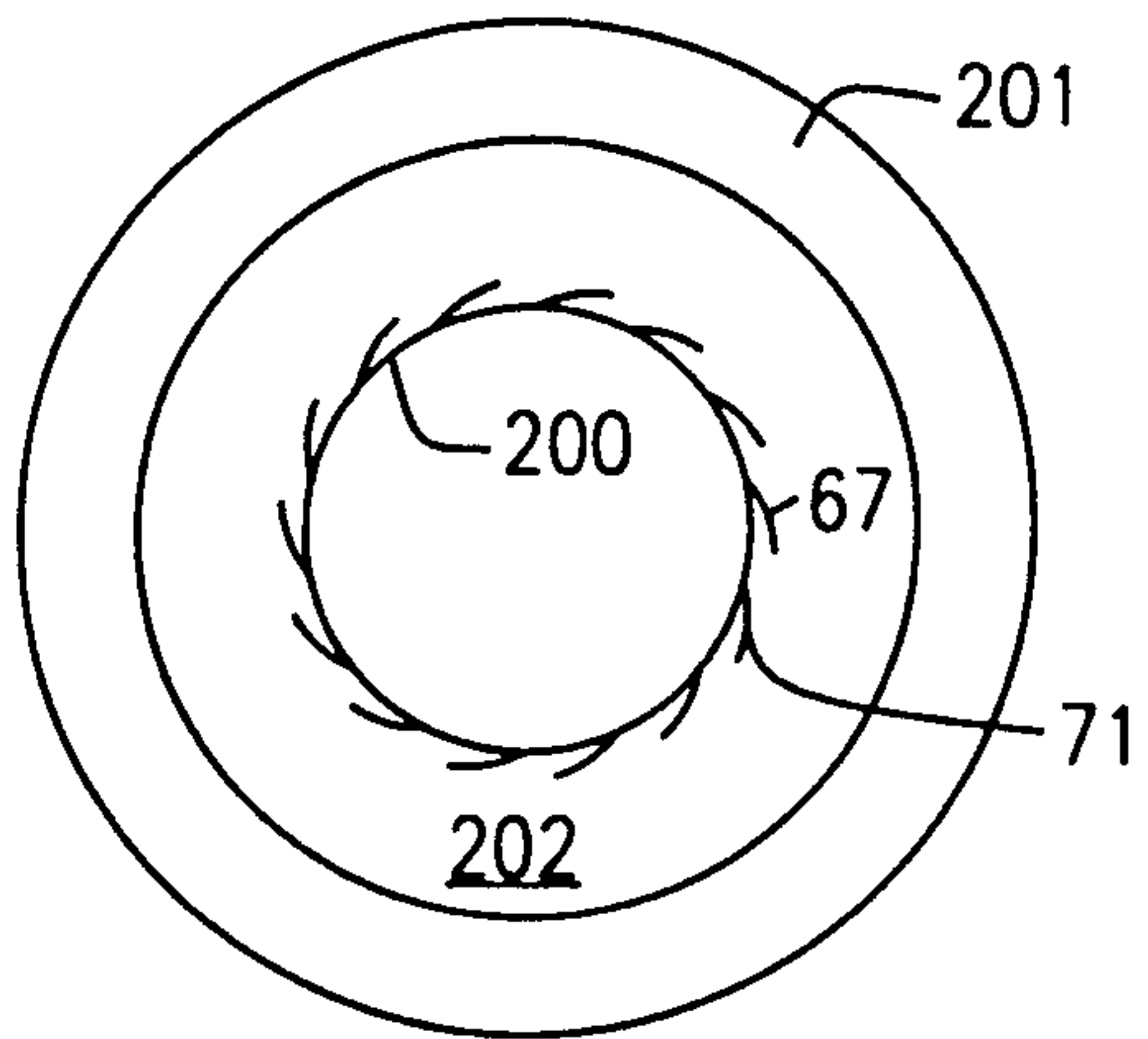


FIG. 21

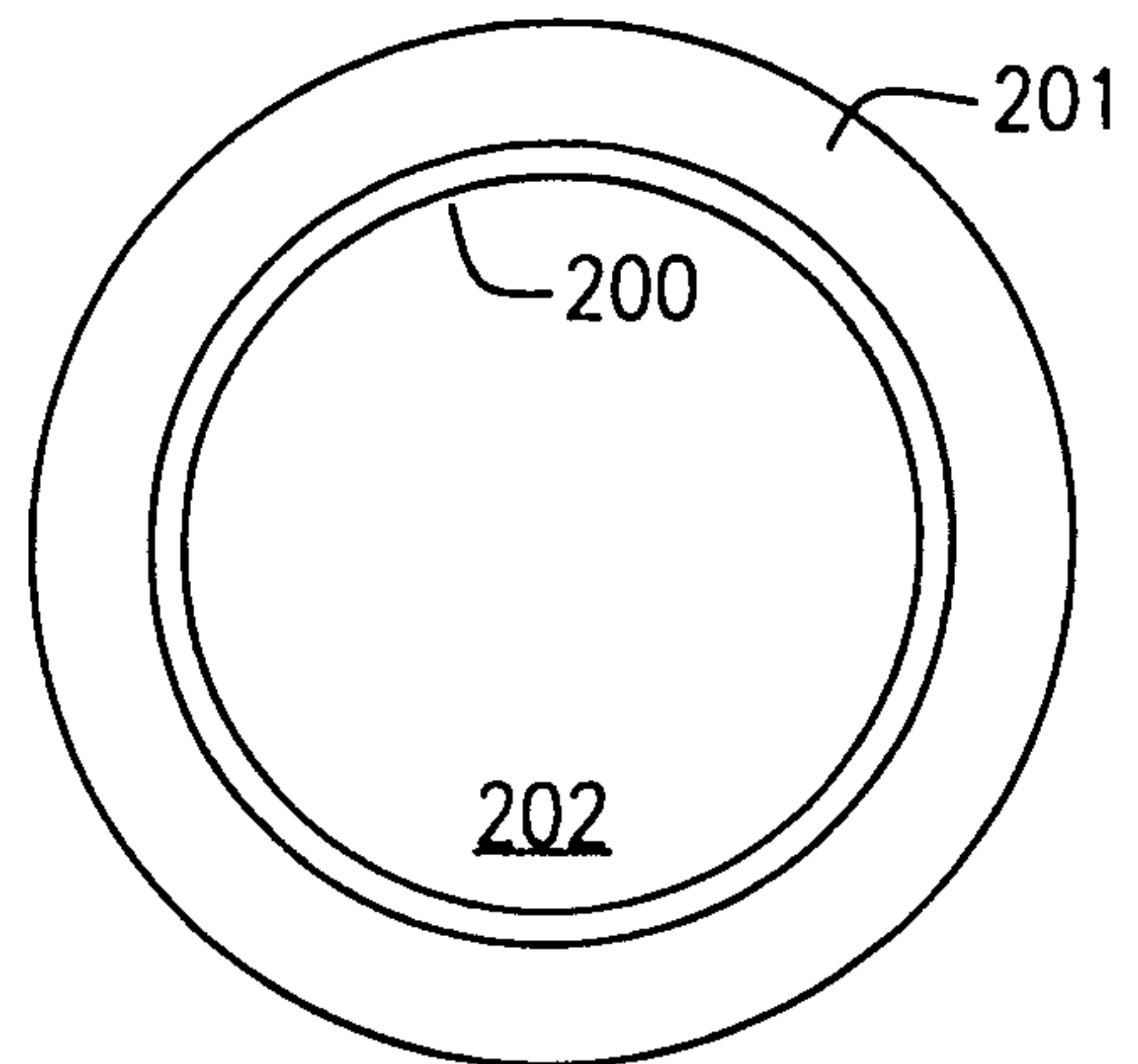


FIG. 22

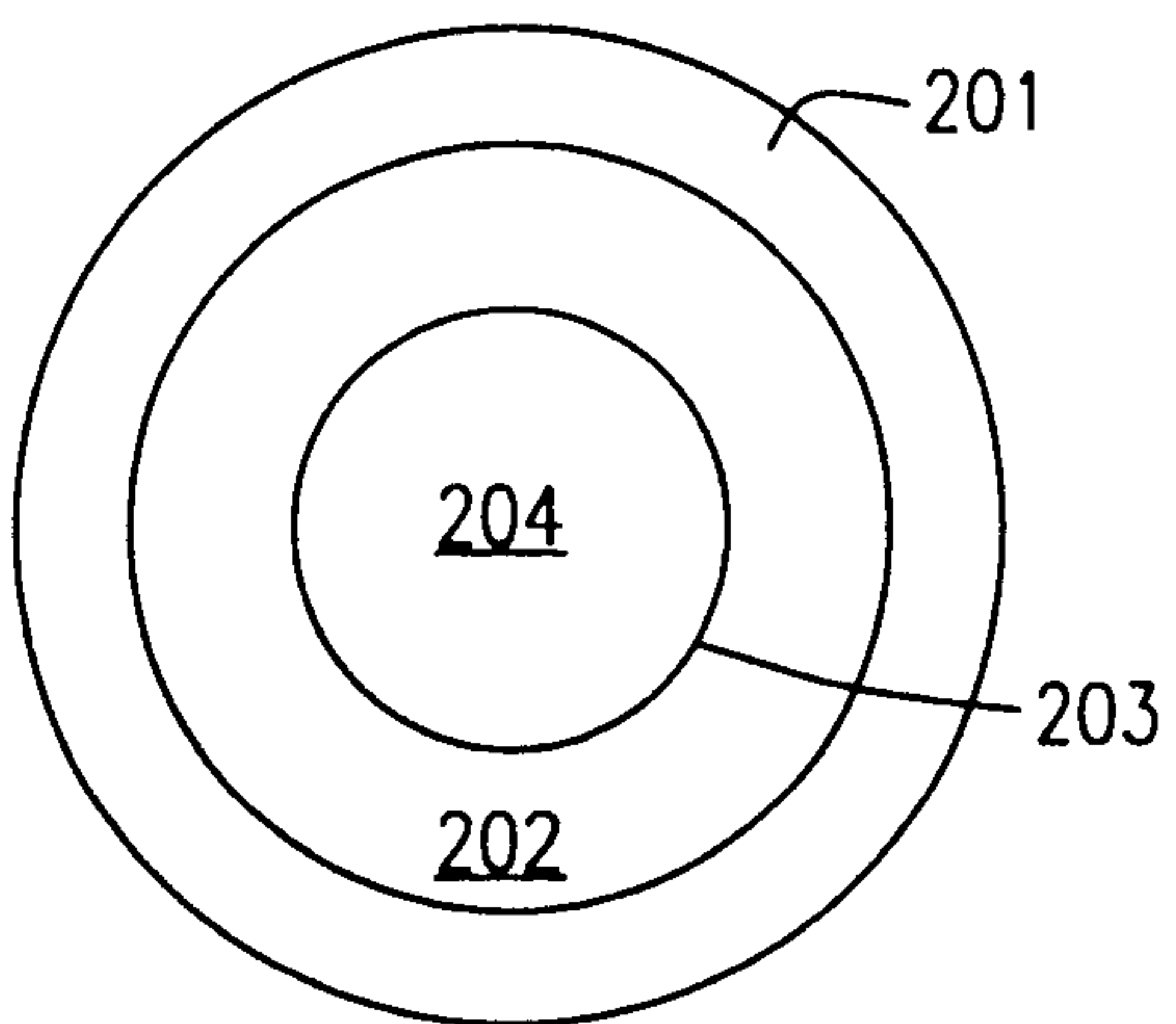


FIG. 23

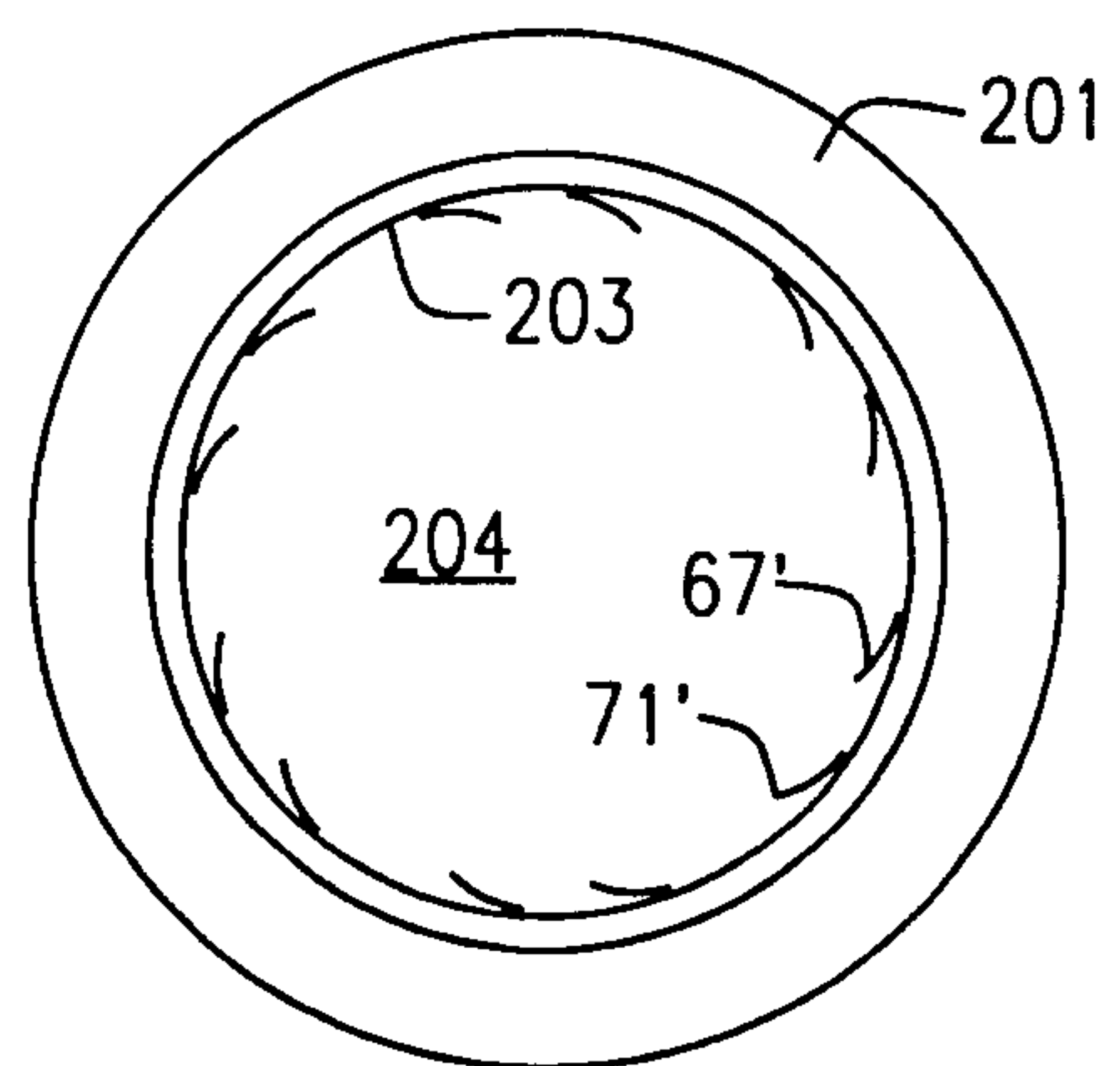


FIG. 24

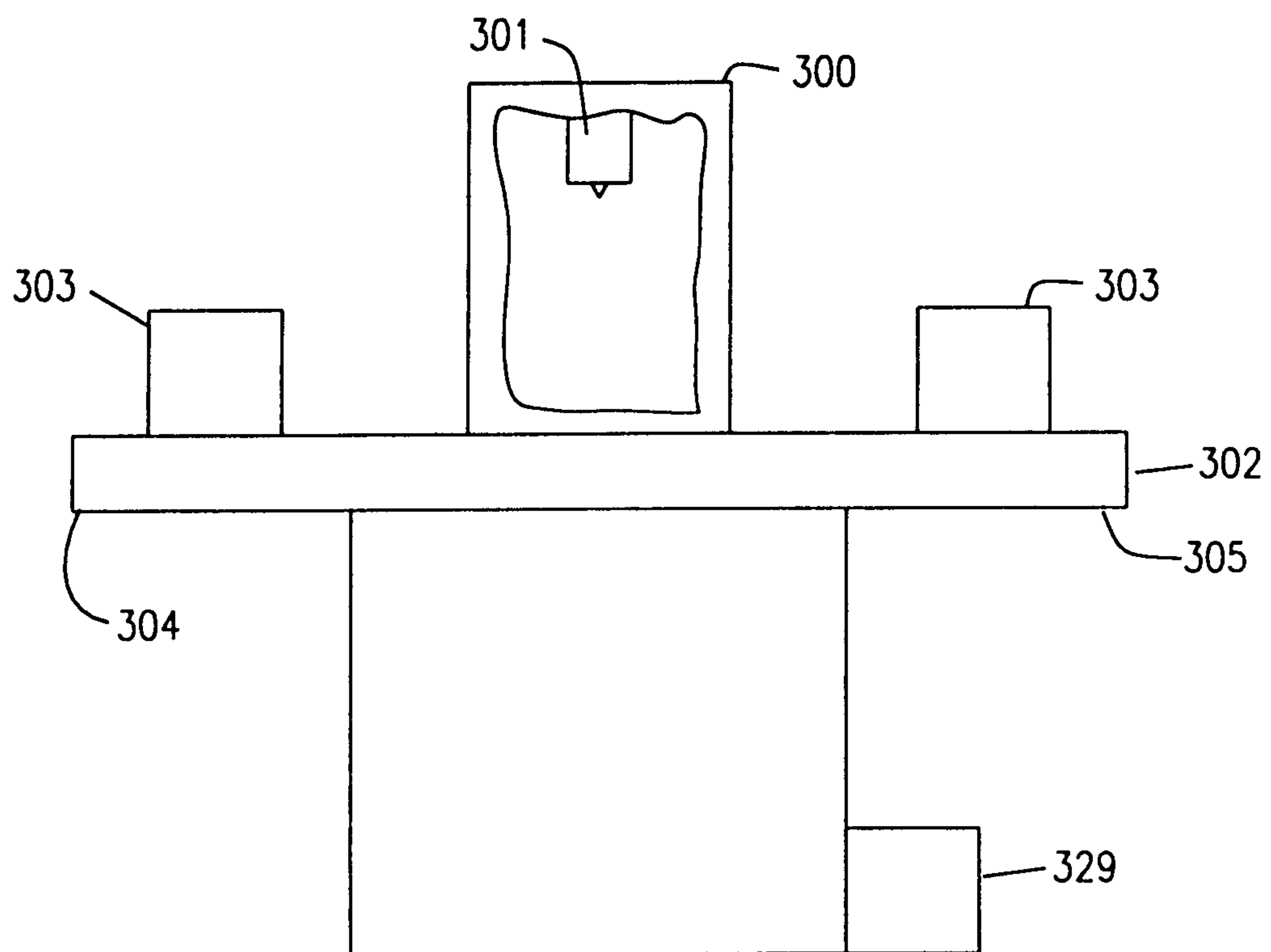


FIG. 25

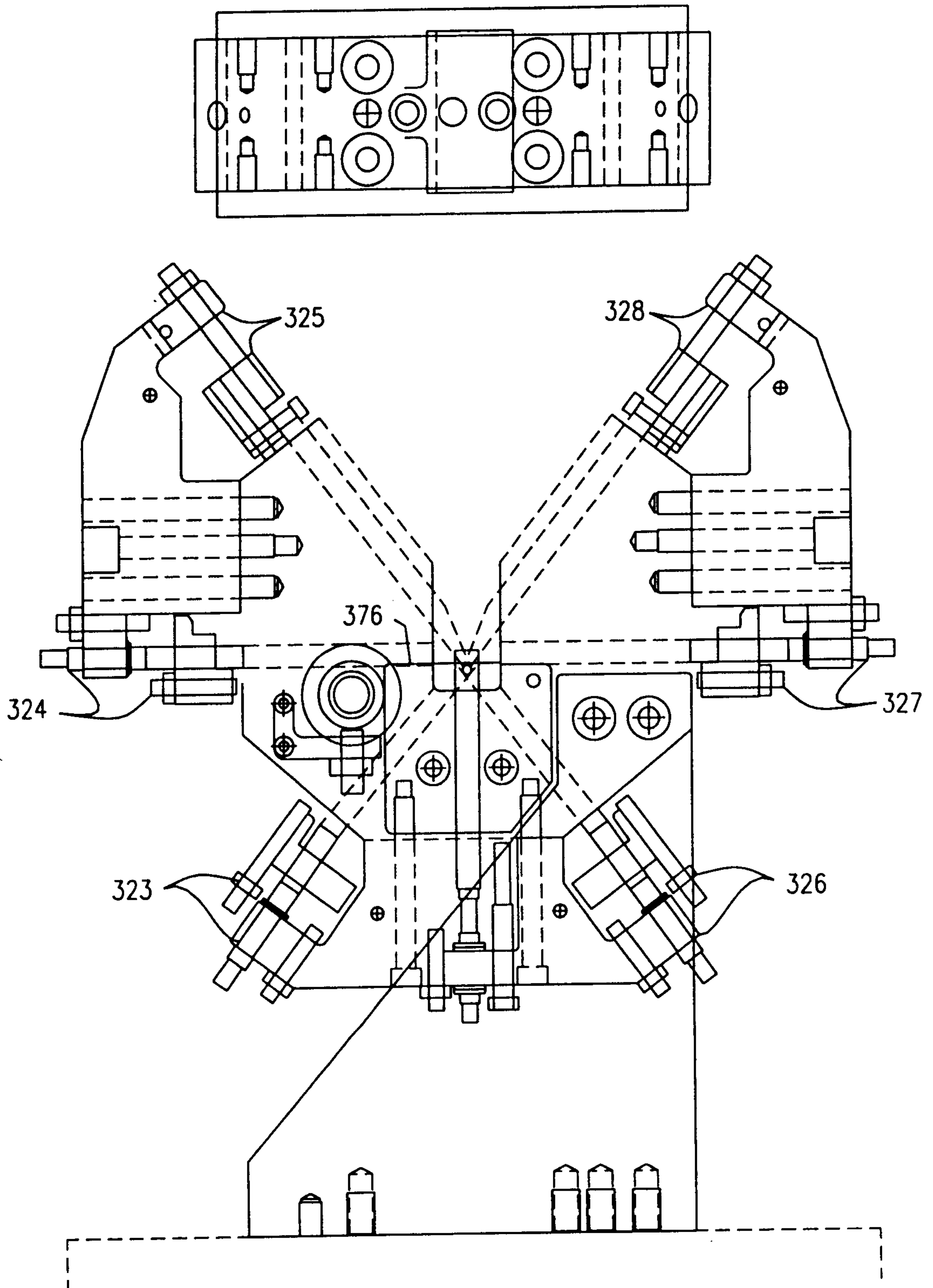


FIG. 26

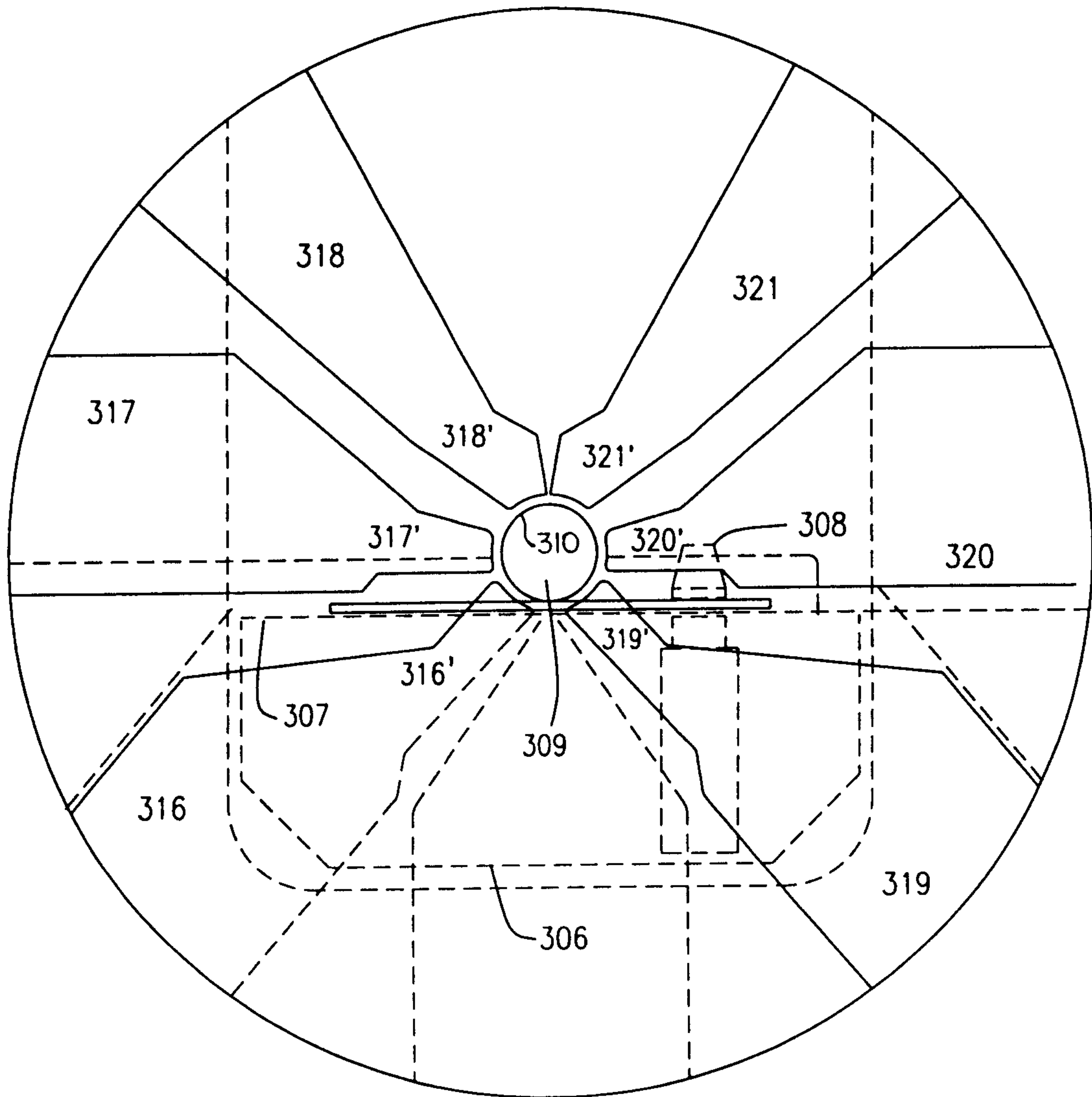


FIG. 27

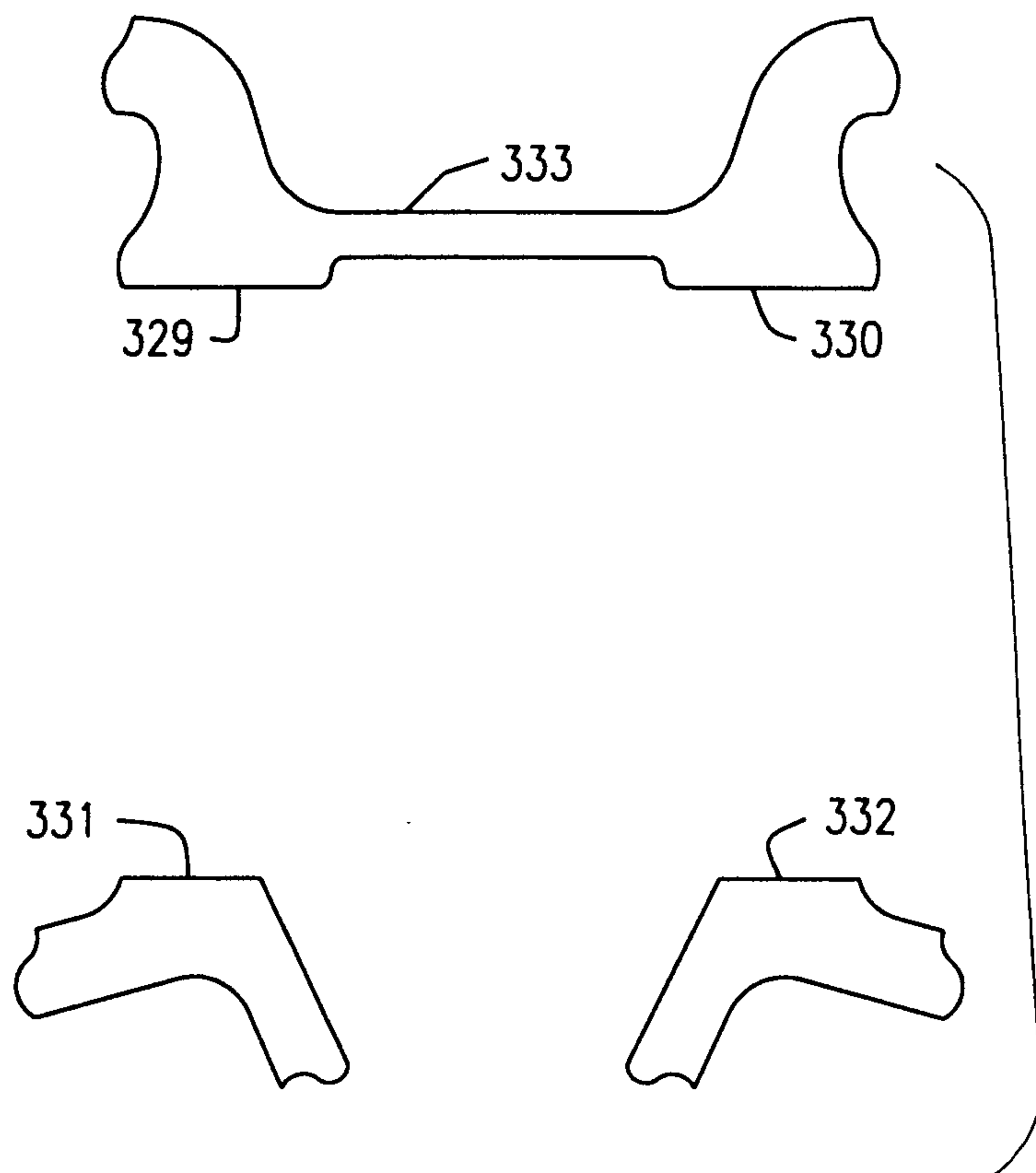


FIG. 28

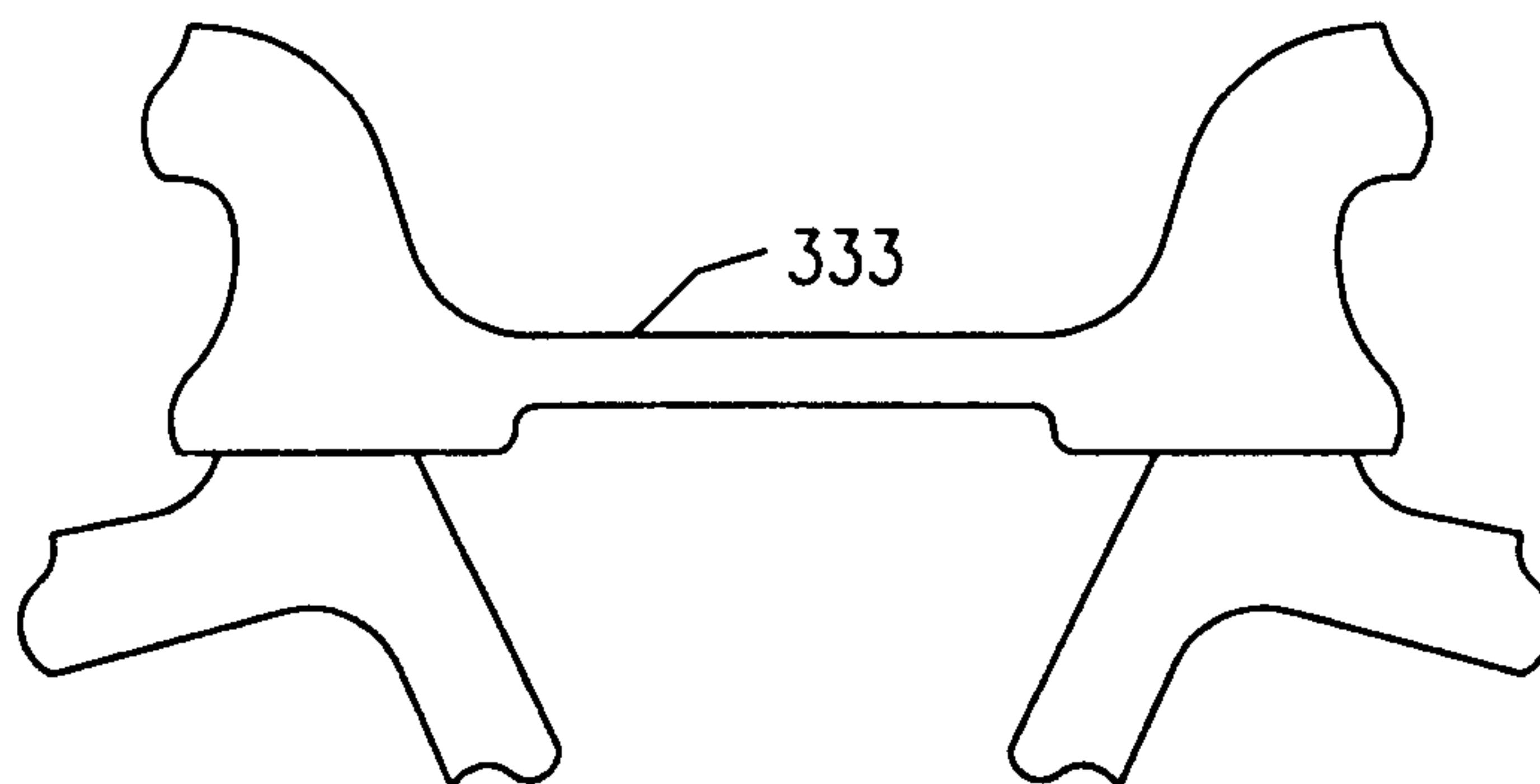


FIG. 29

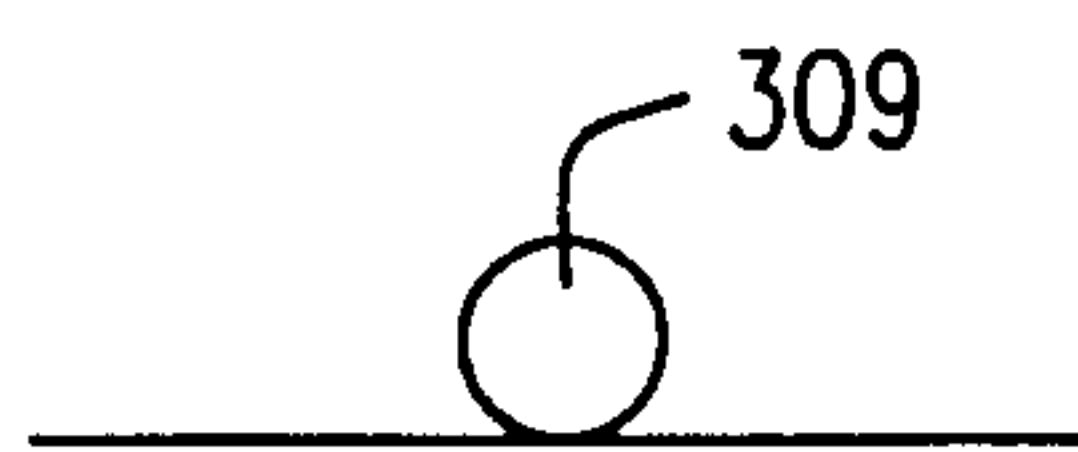


FIG. 30A

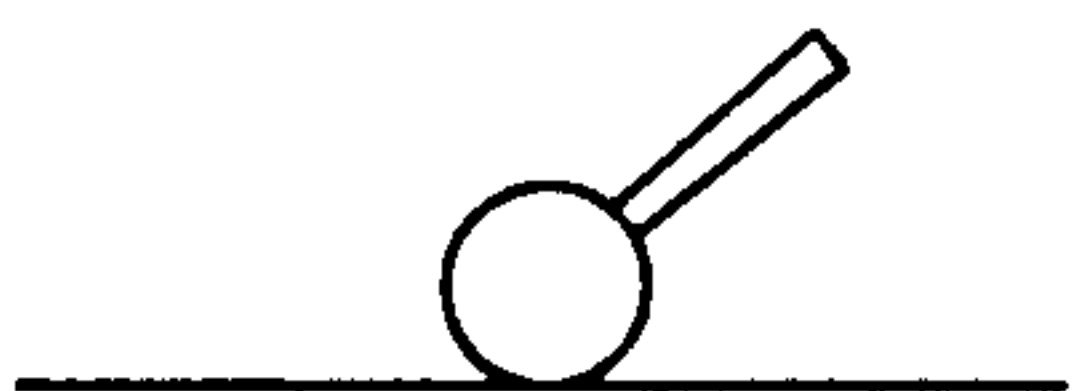


FIG. 30B

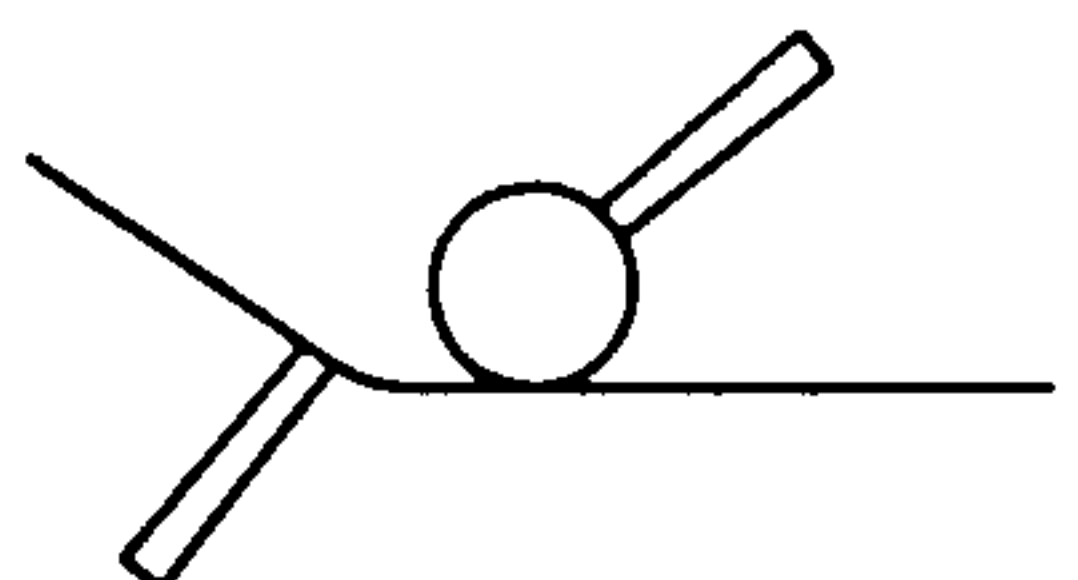


FIG. 30C

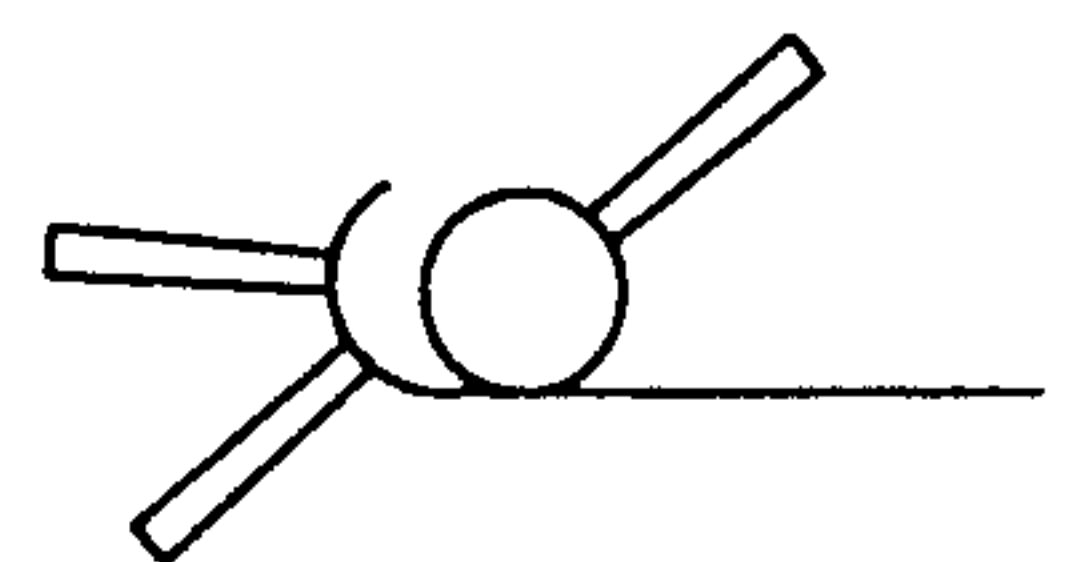


FIG. 30D

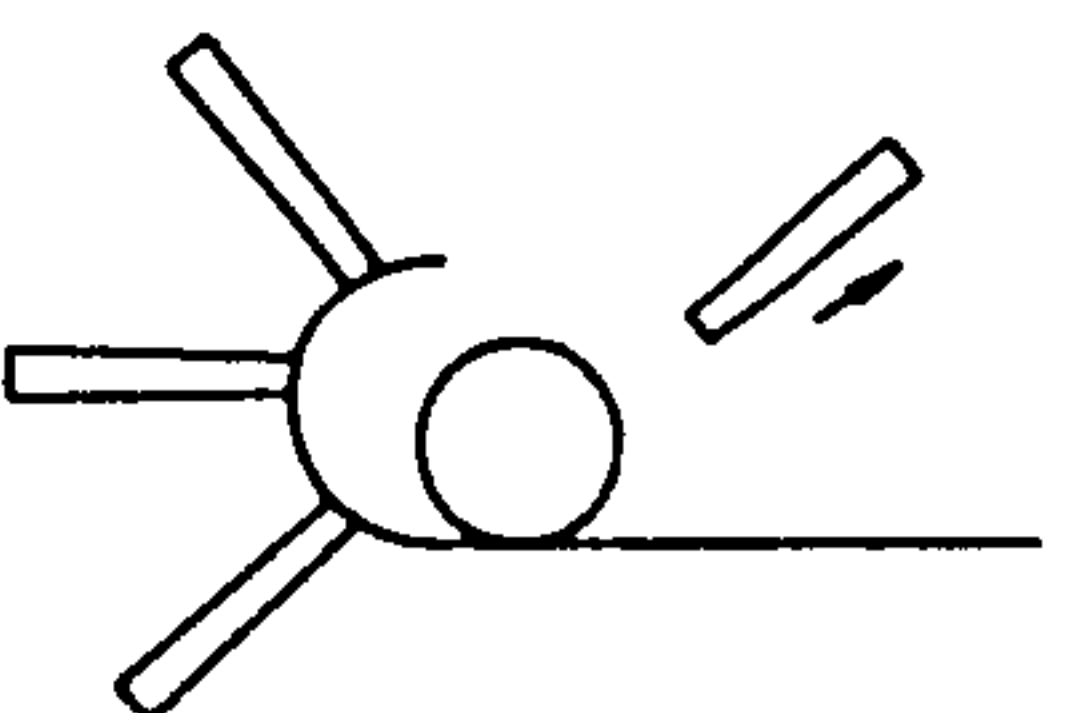


FIG. 30E

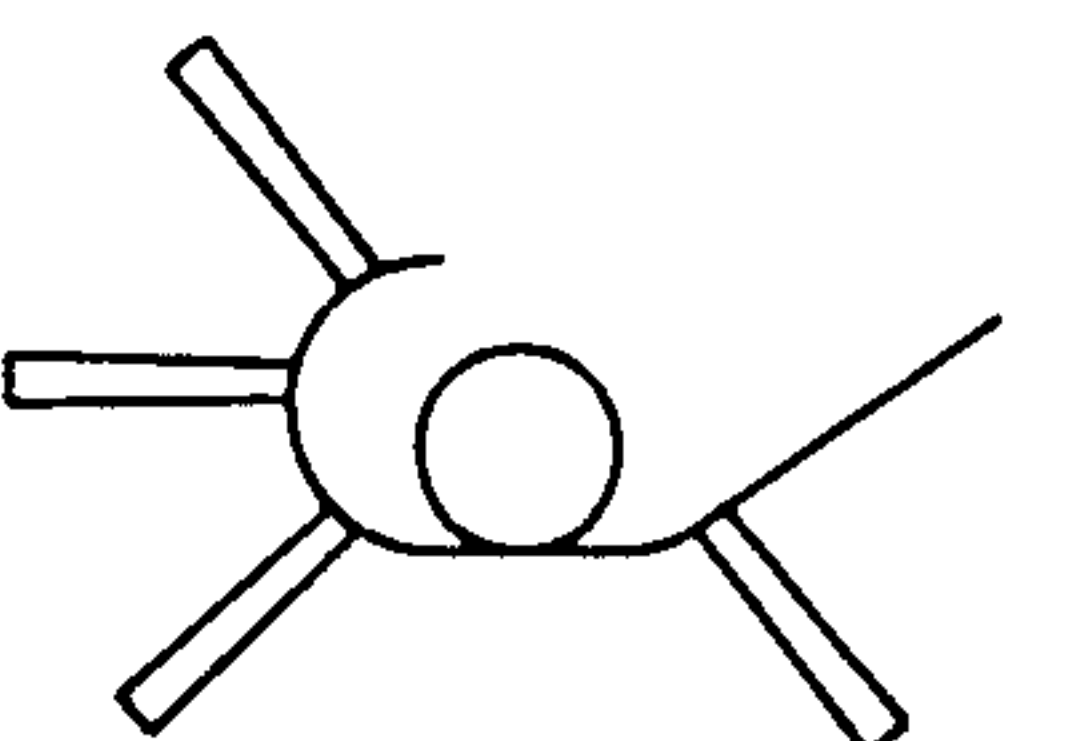


FIG. 30F

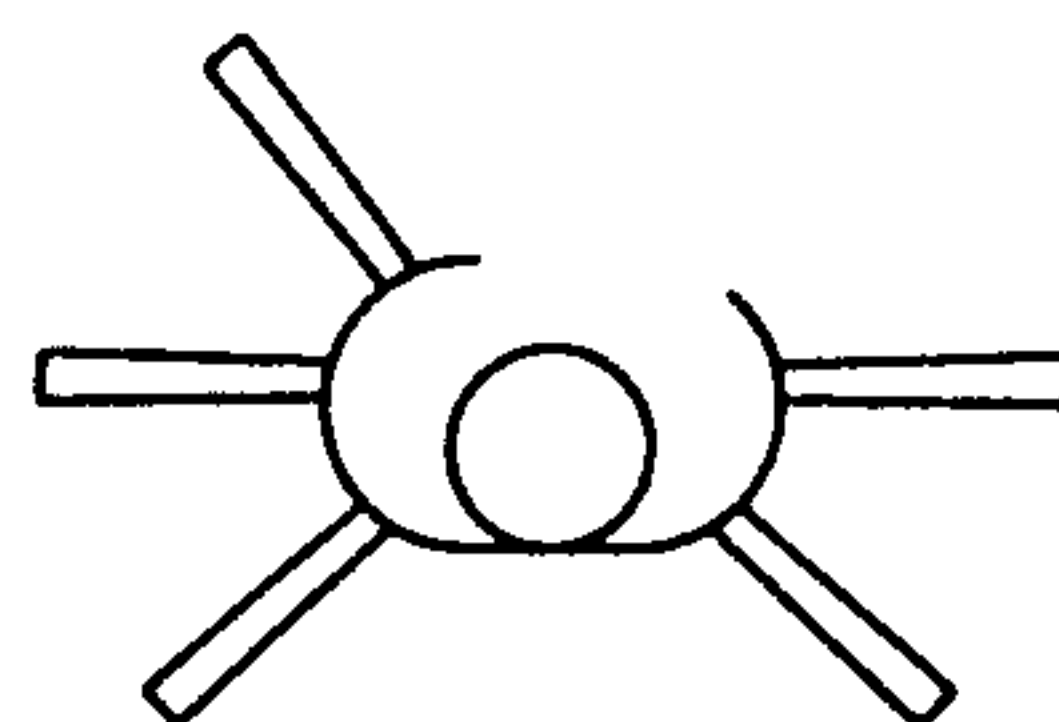


FIG. 30G

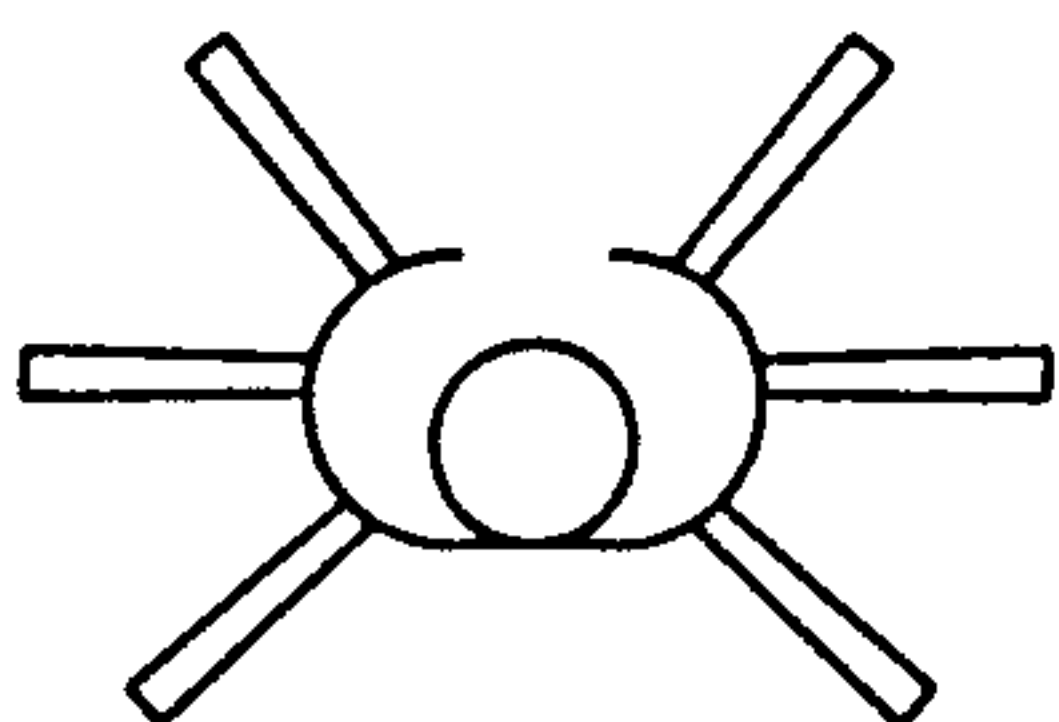


FIG. 30H

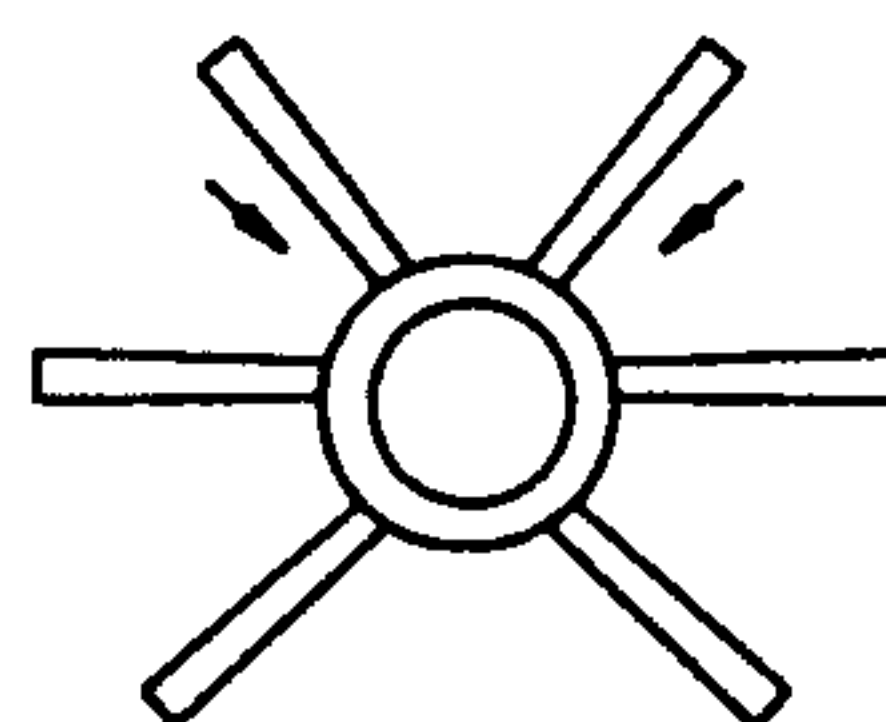


FIG. 30I

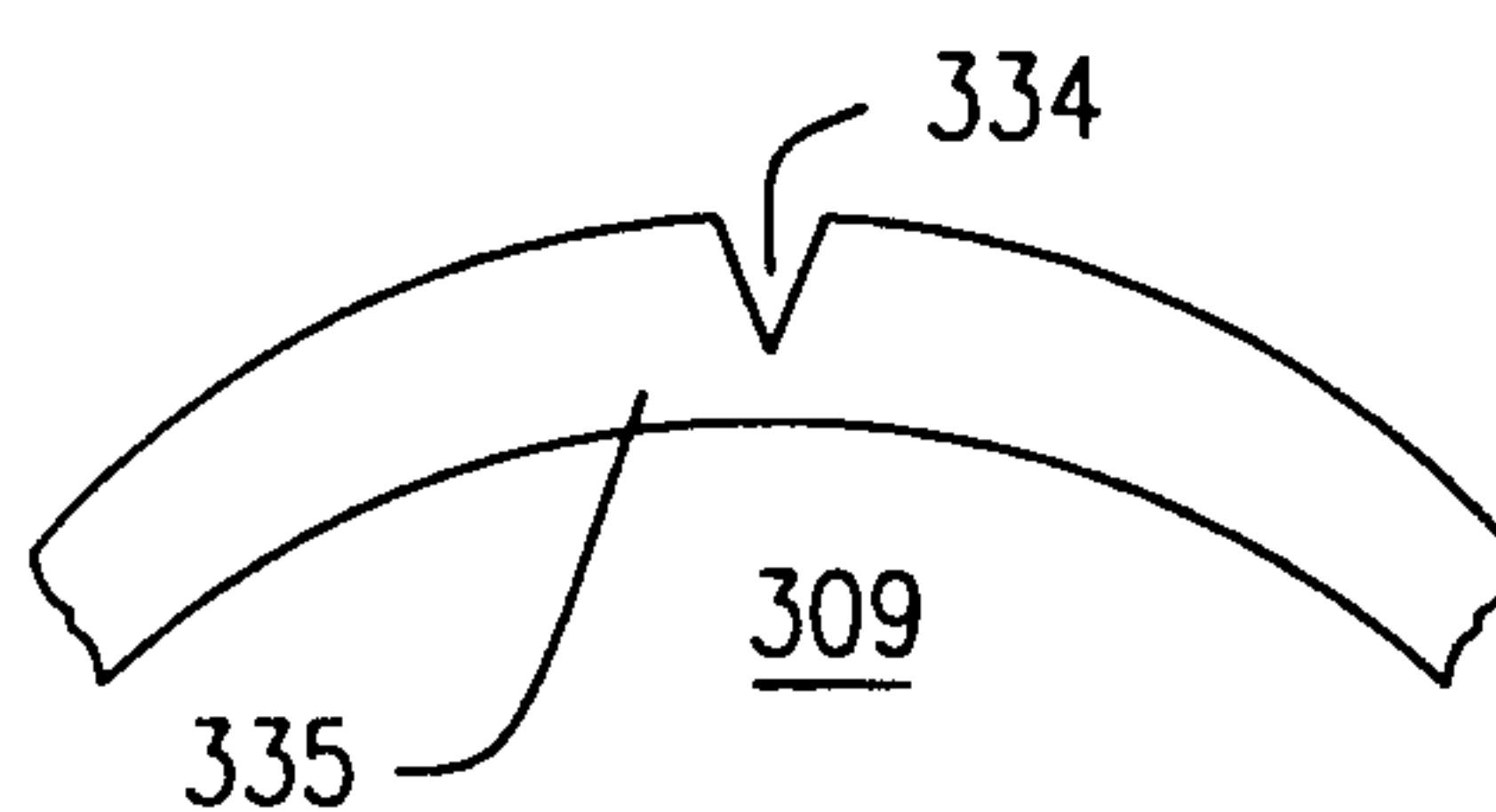


FIG. 31

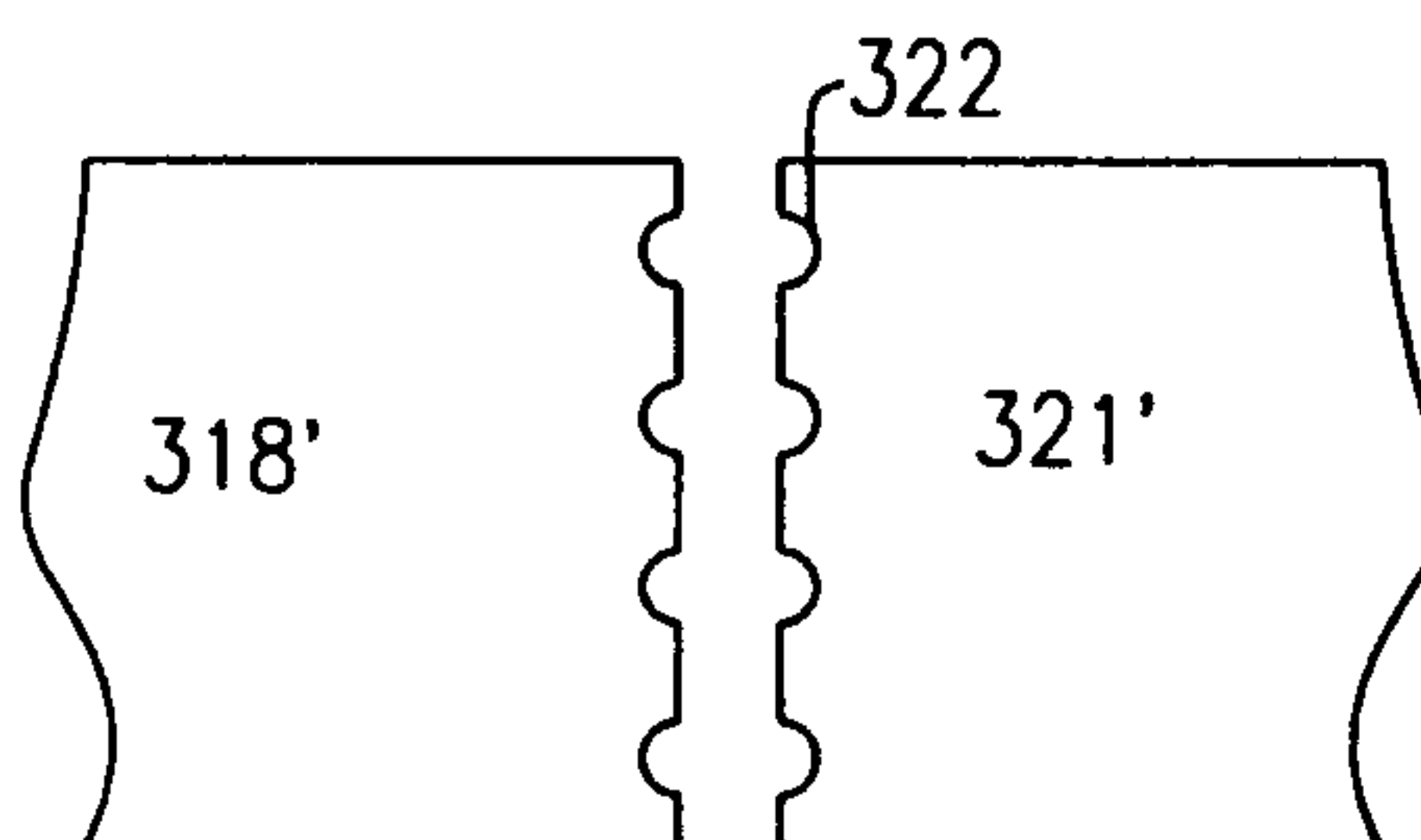
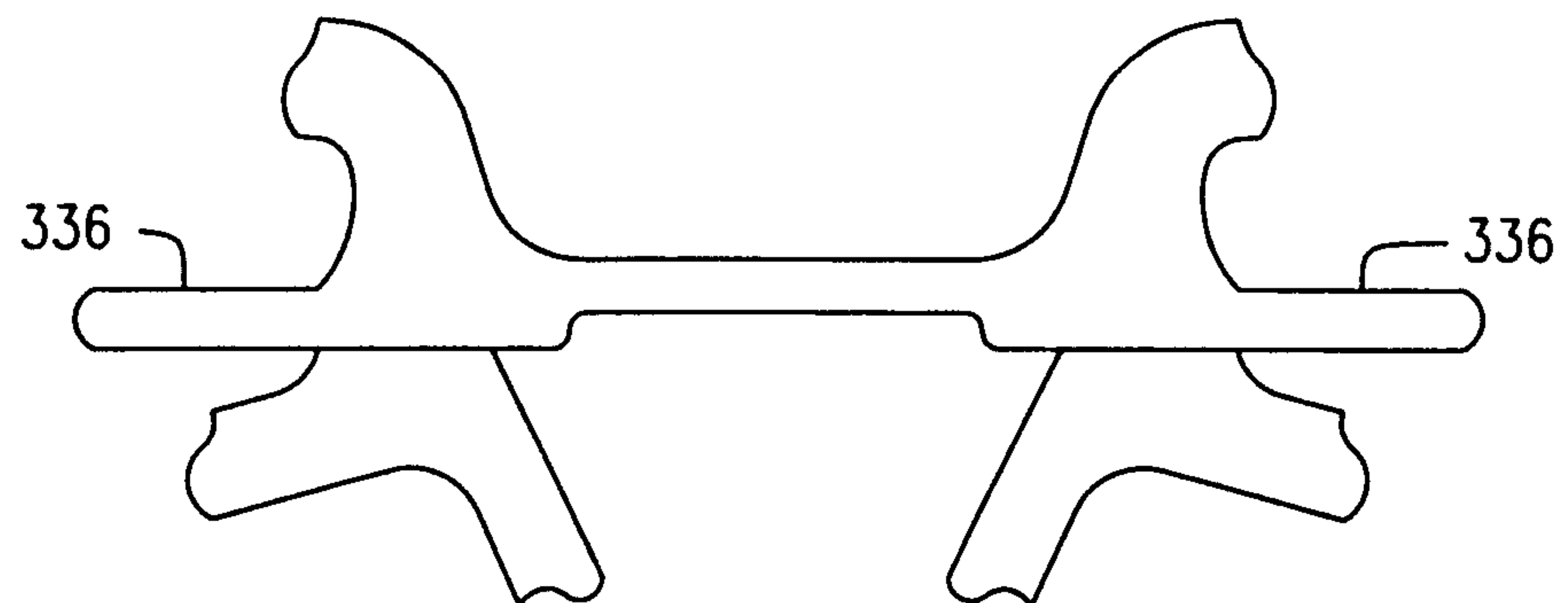
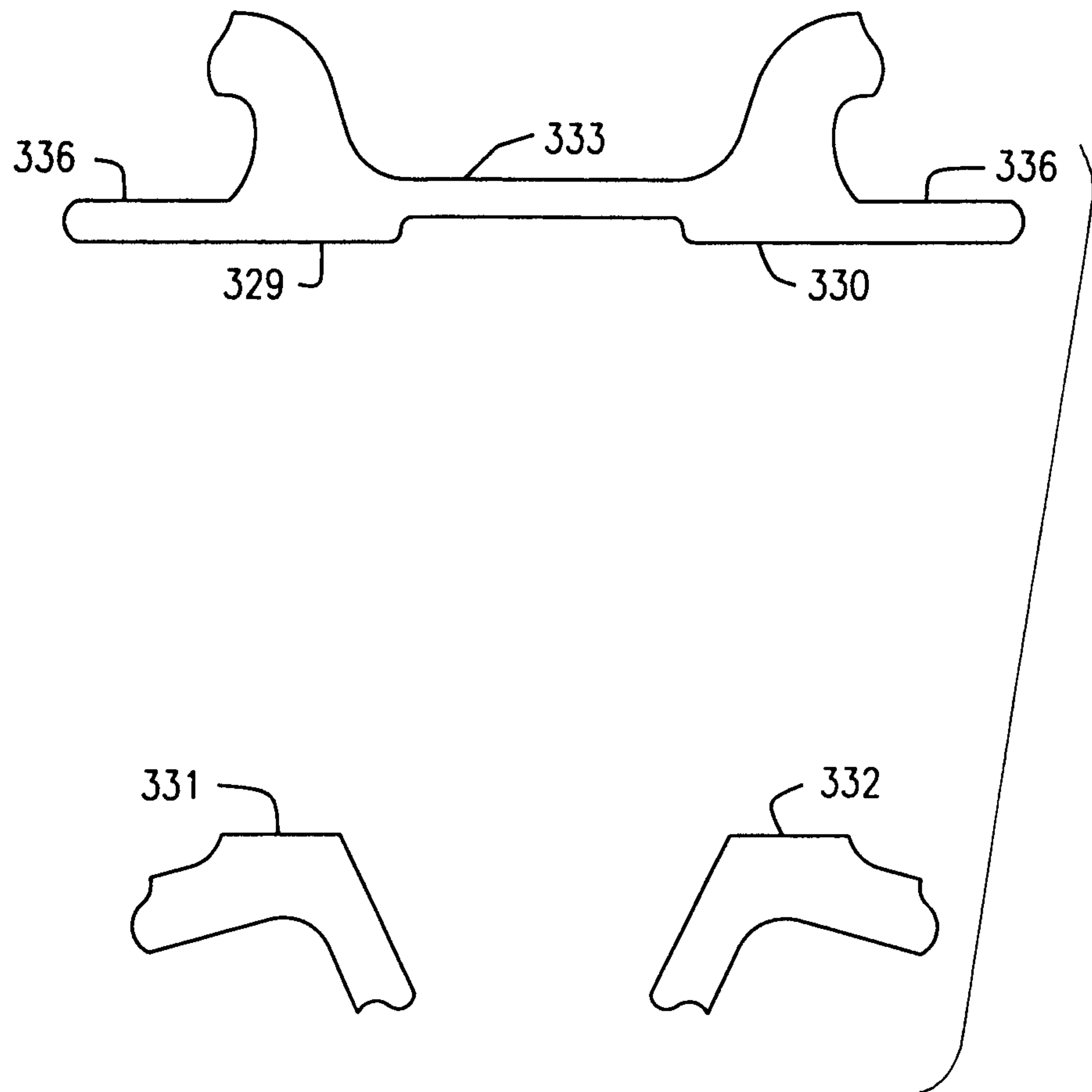


FIG. 32



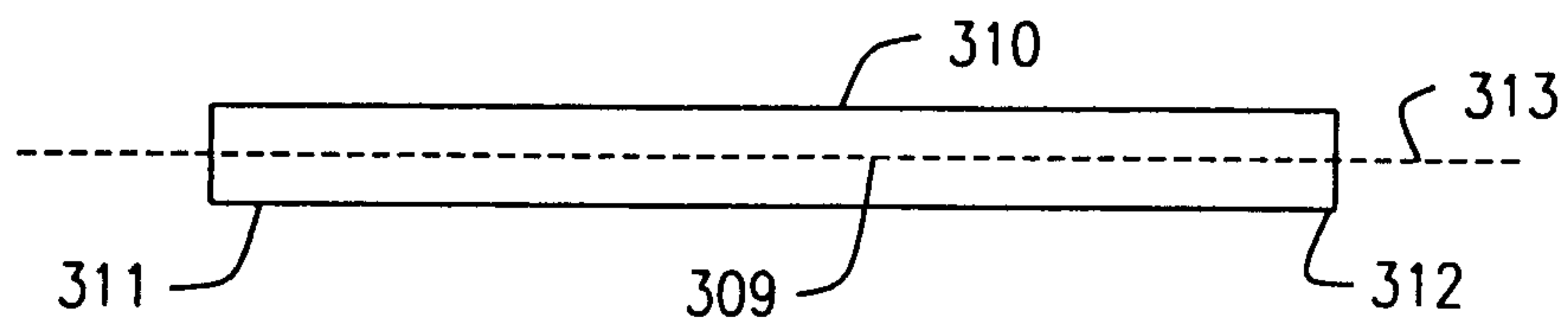


FIG. 35

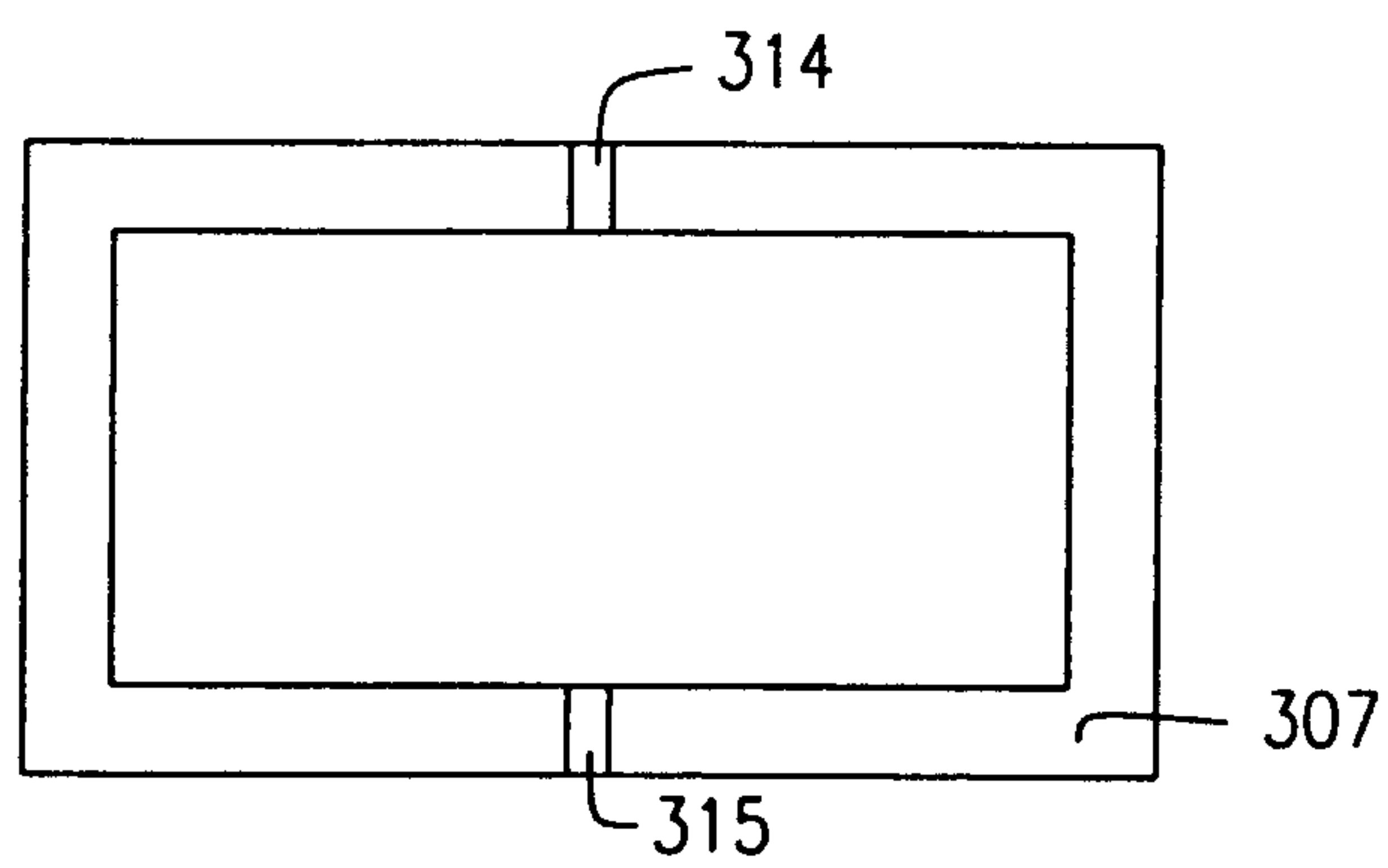
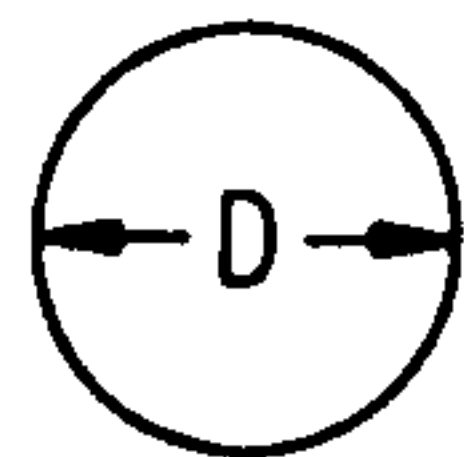
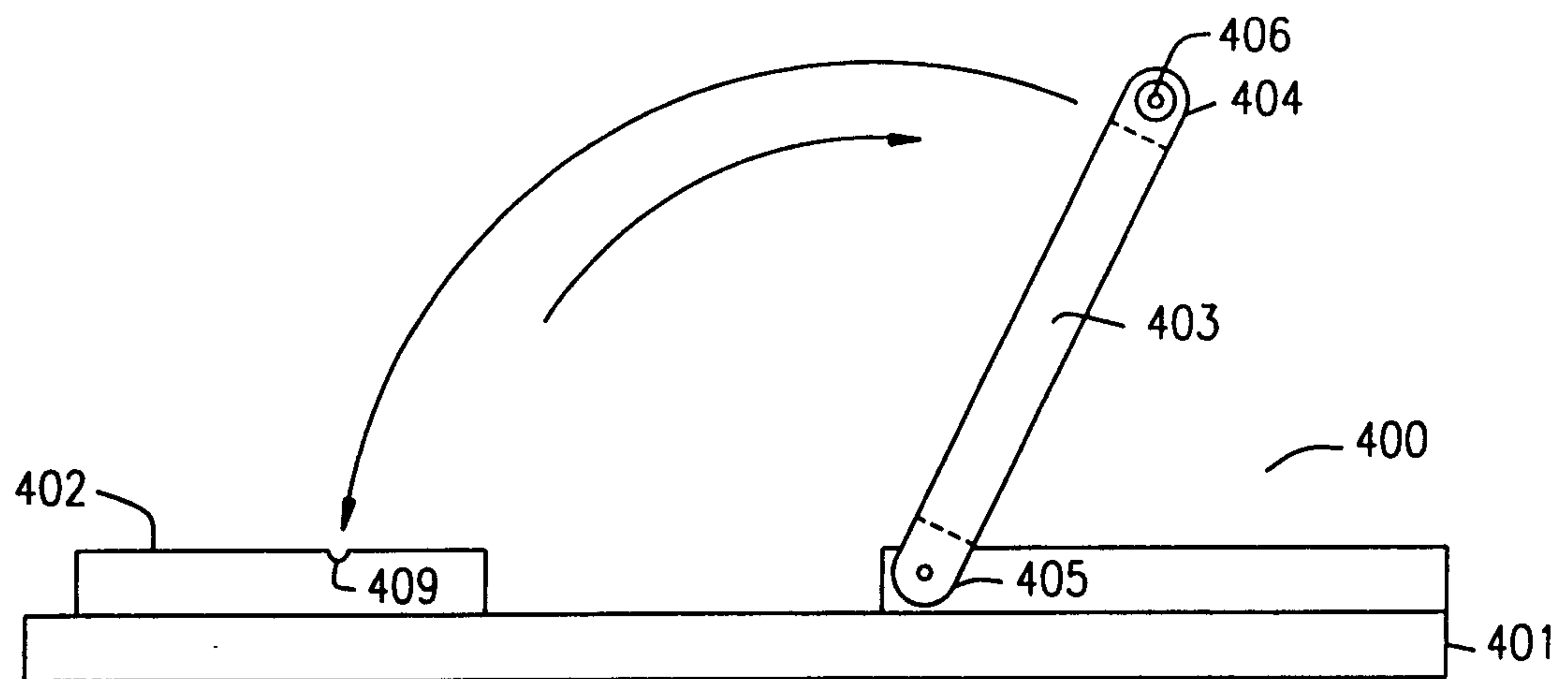
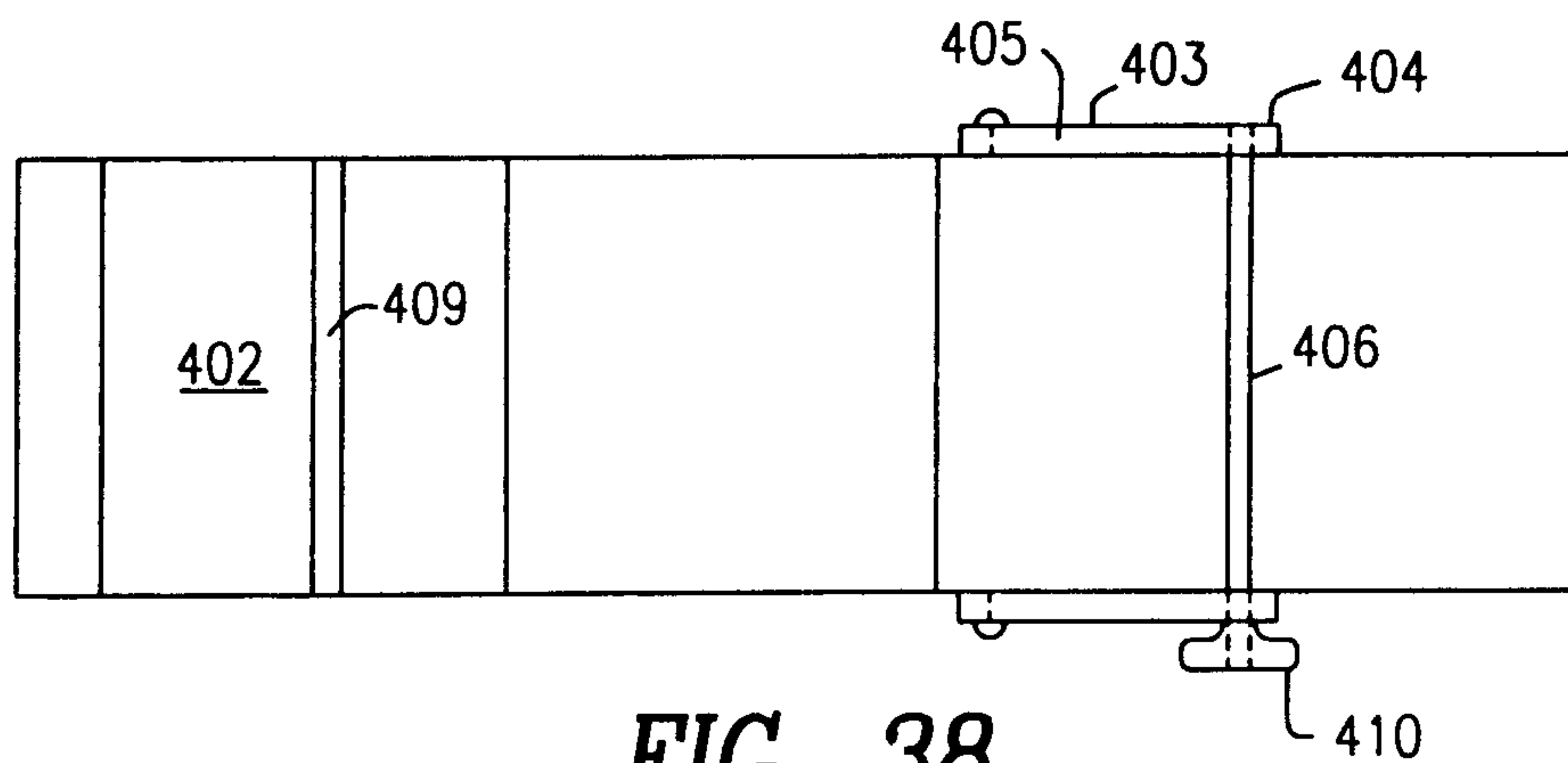
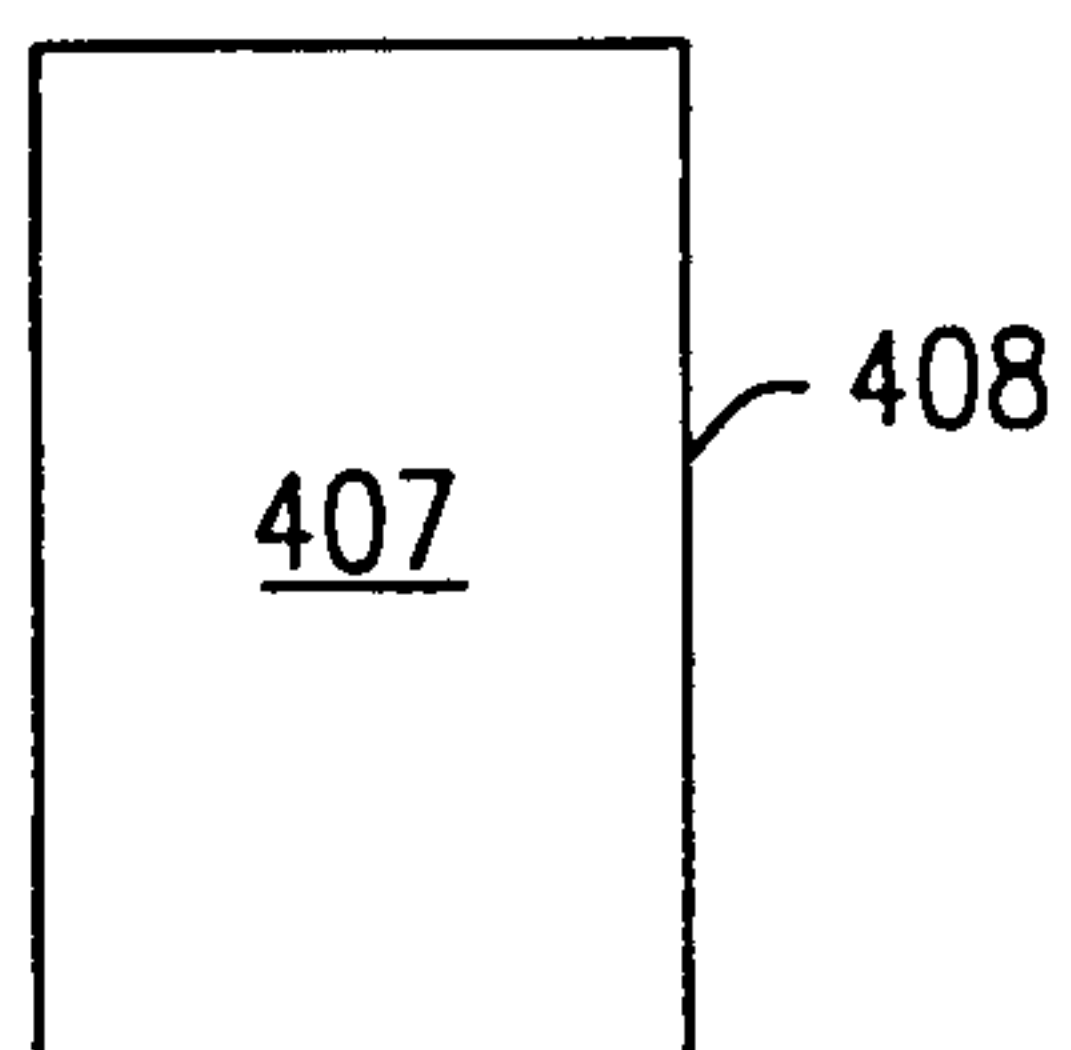
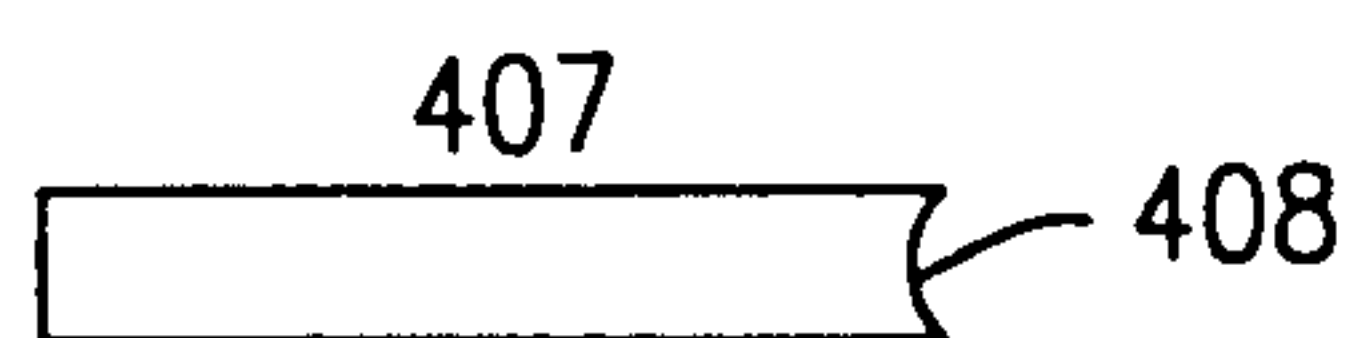
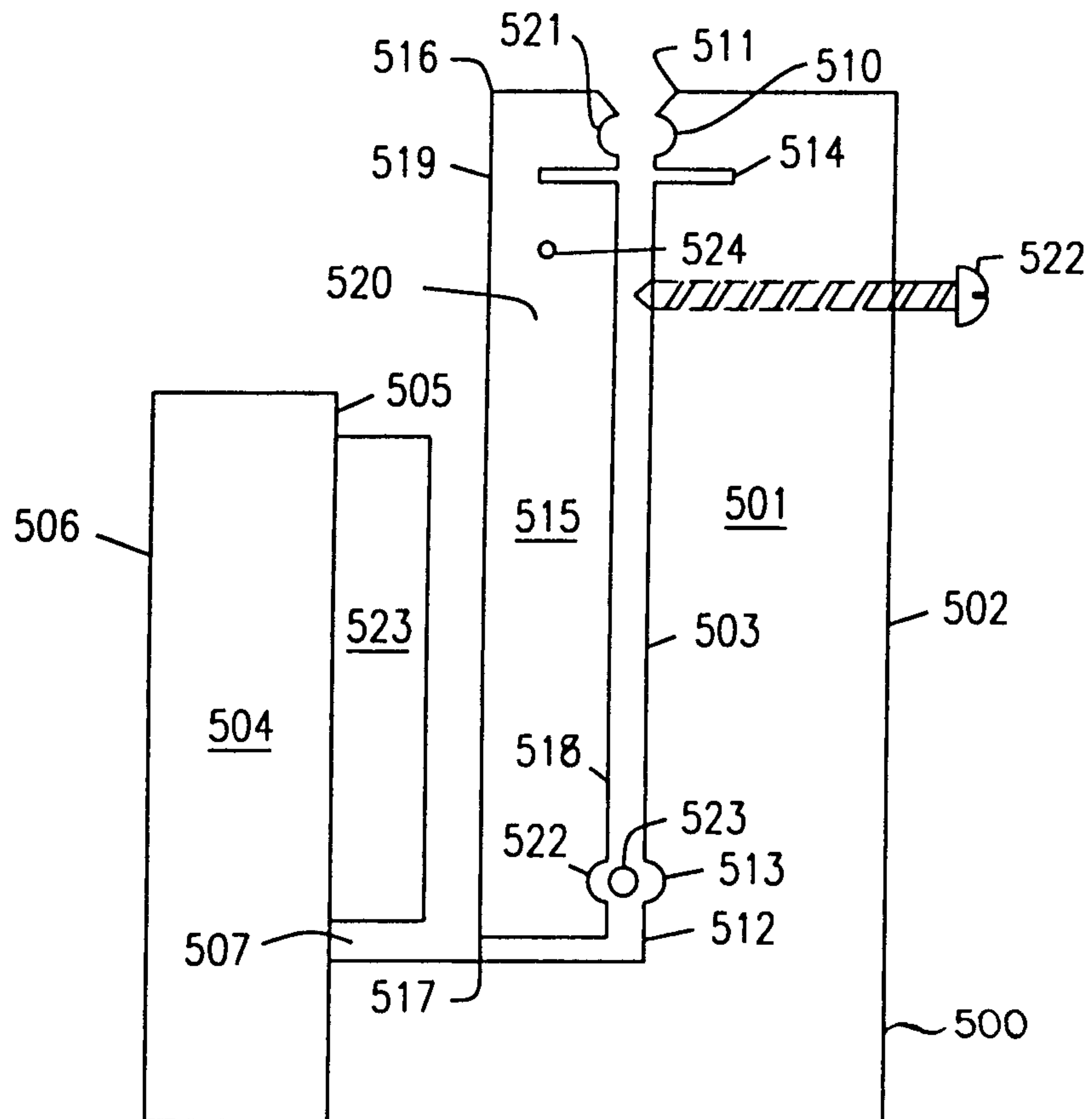
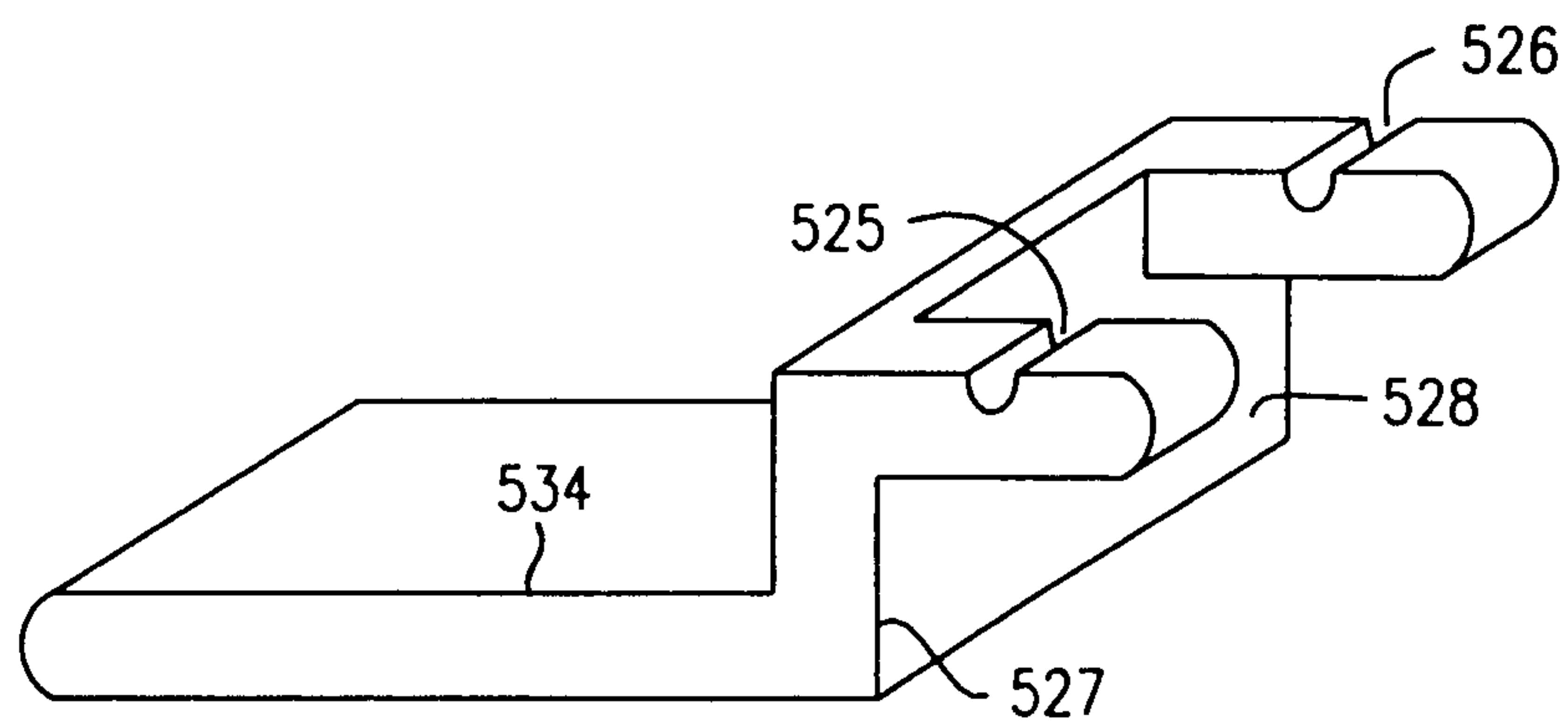


FIG. 36

**FIG. 37****FIG. 38****FIG. 39****FIG. 40**

**FIG. 41****FIG. 42**

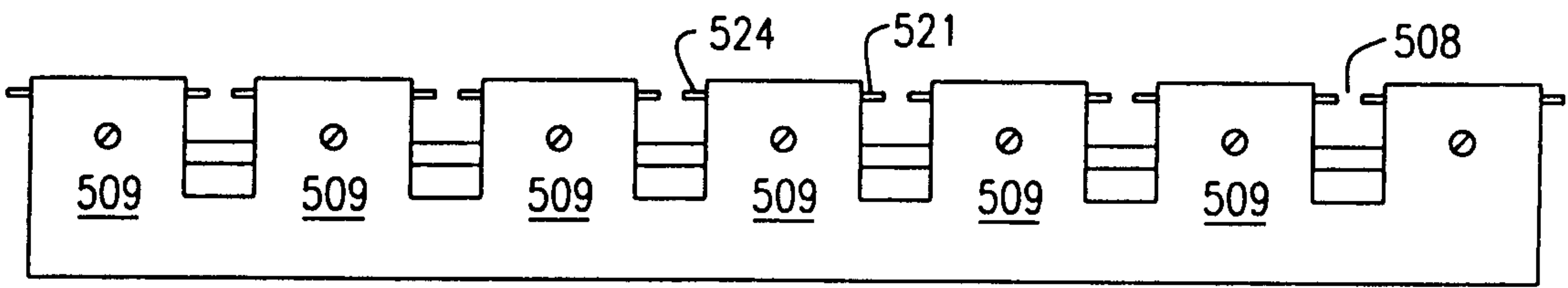


FIG. 43

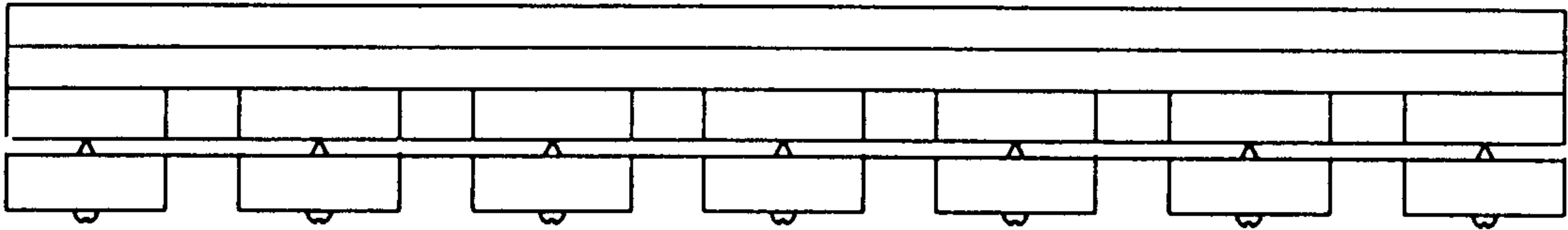


FIG. 44

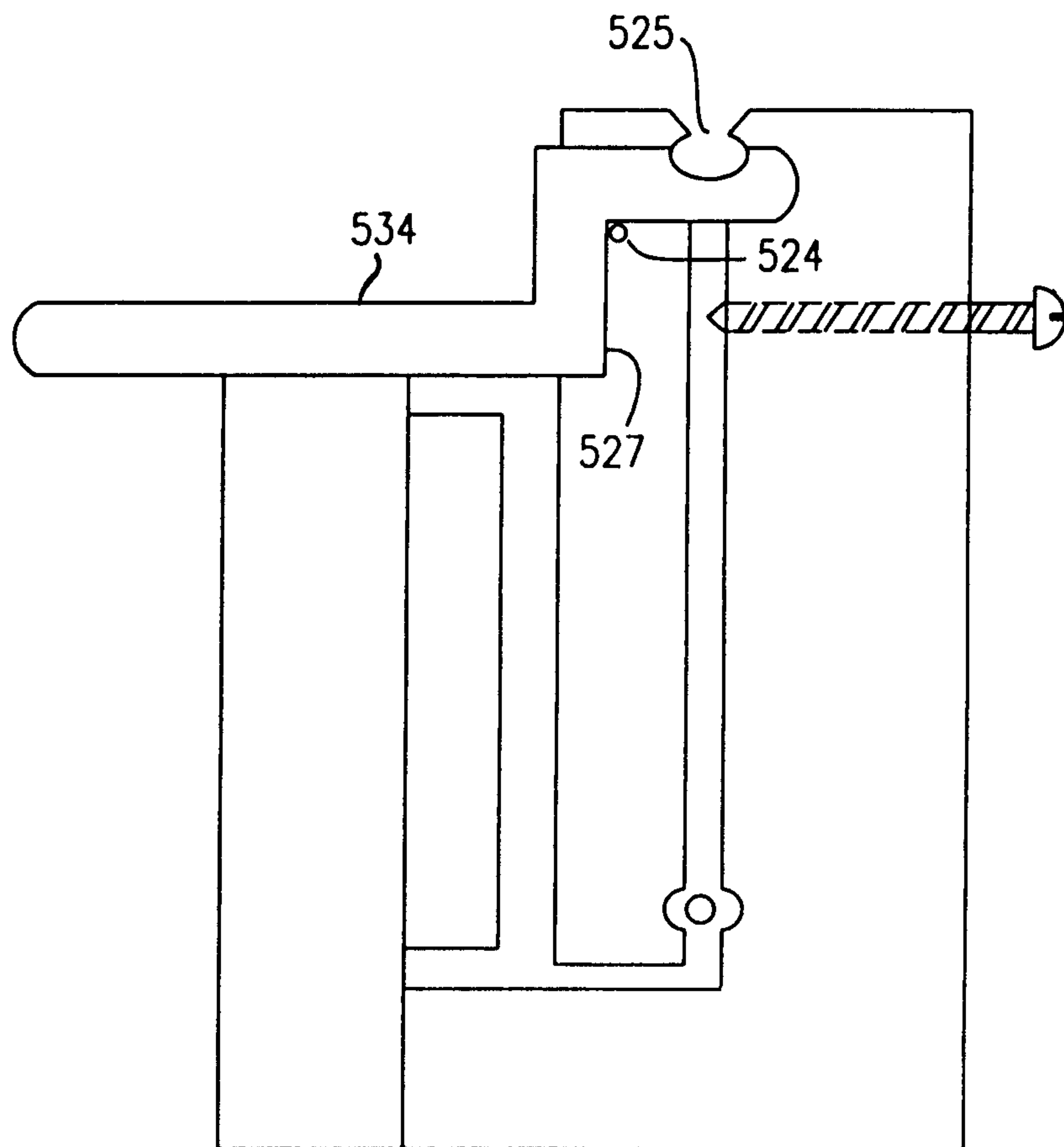


FIG. 45

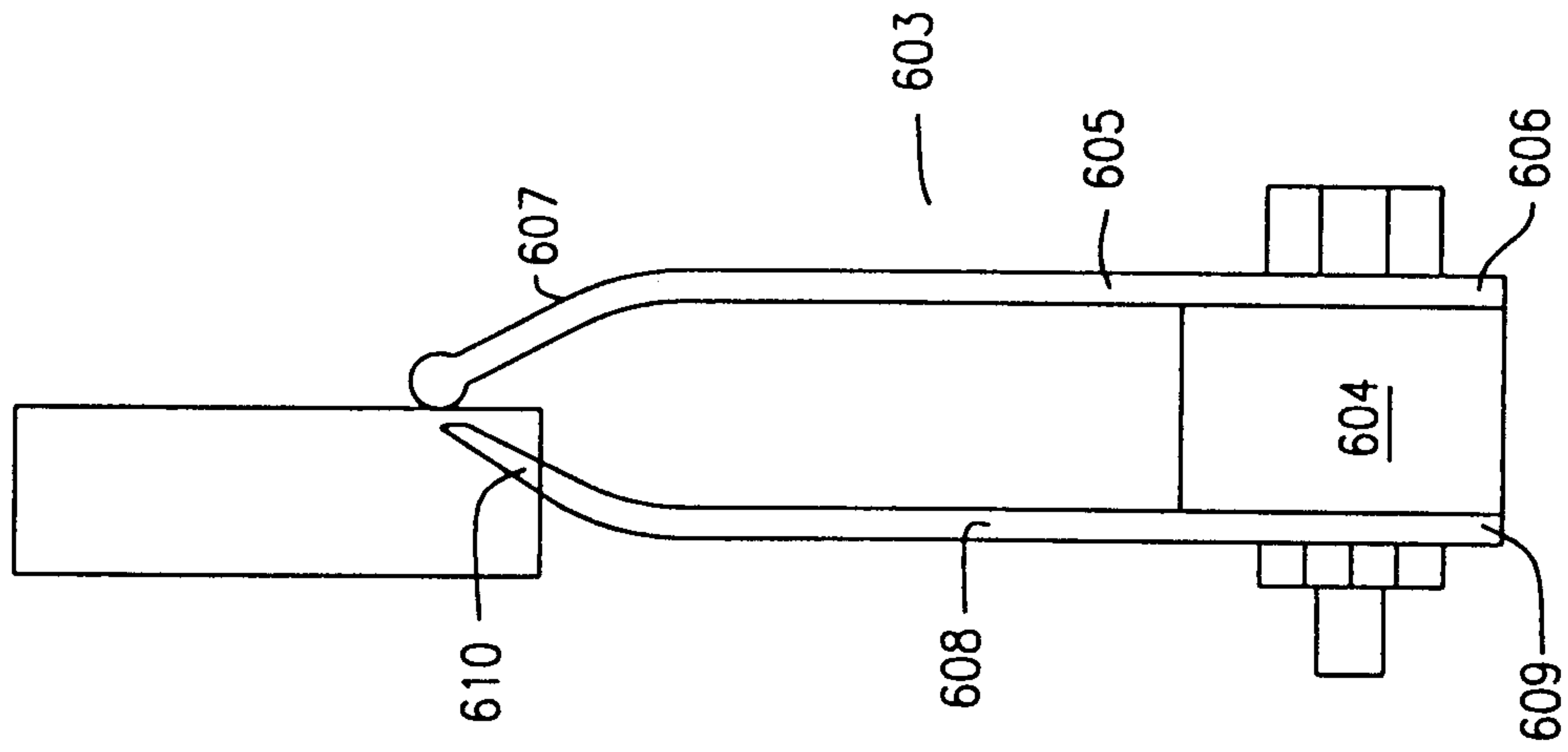


FIG. 46

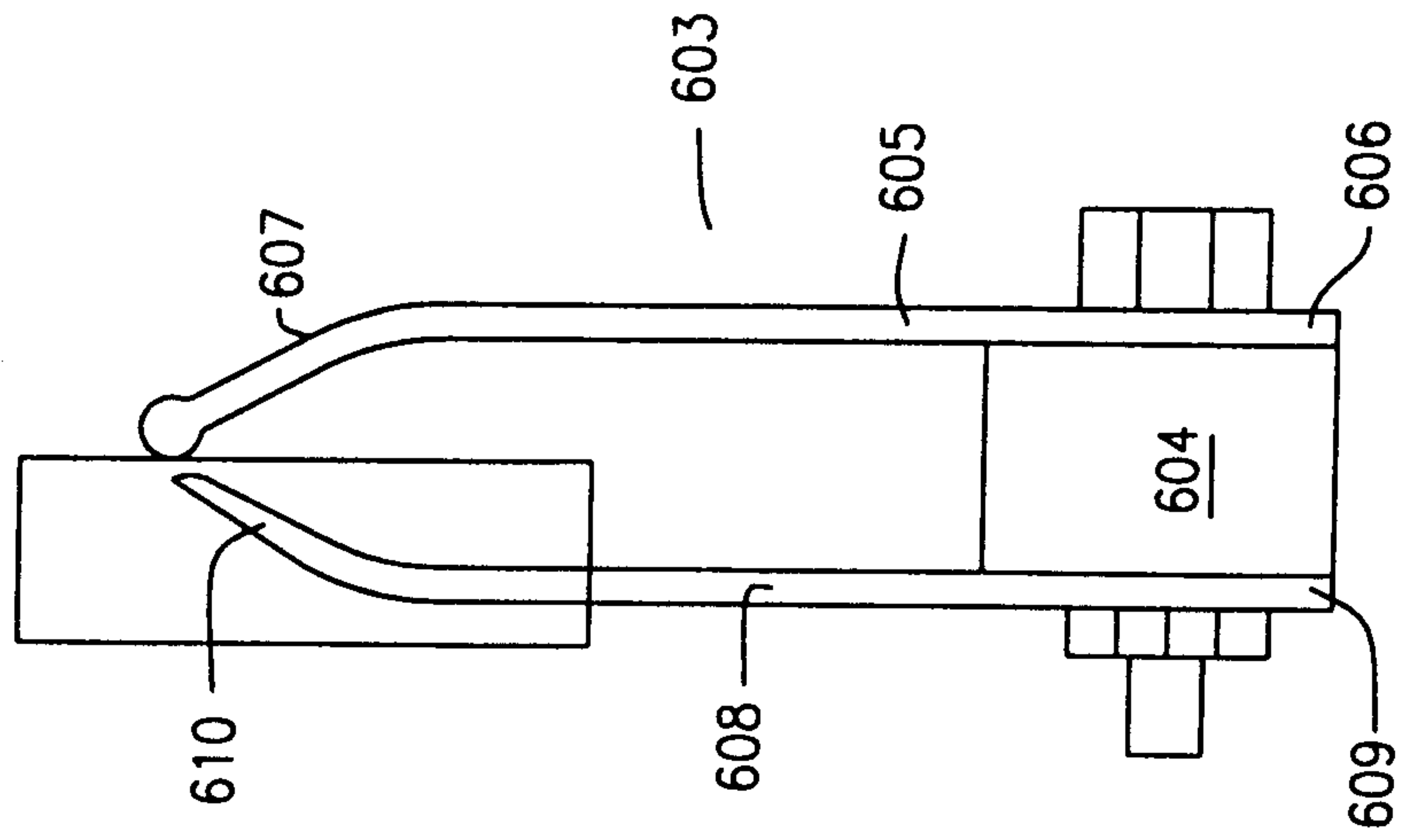


FIG. 47

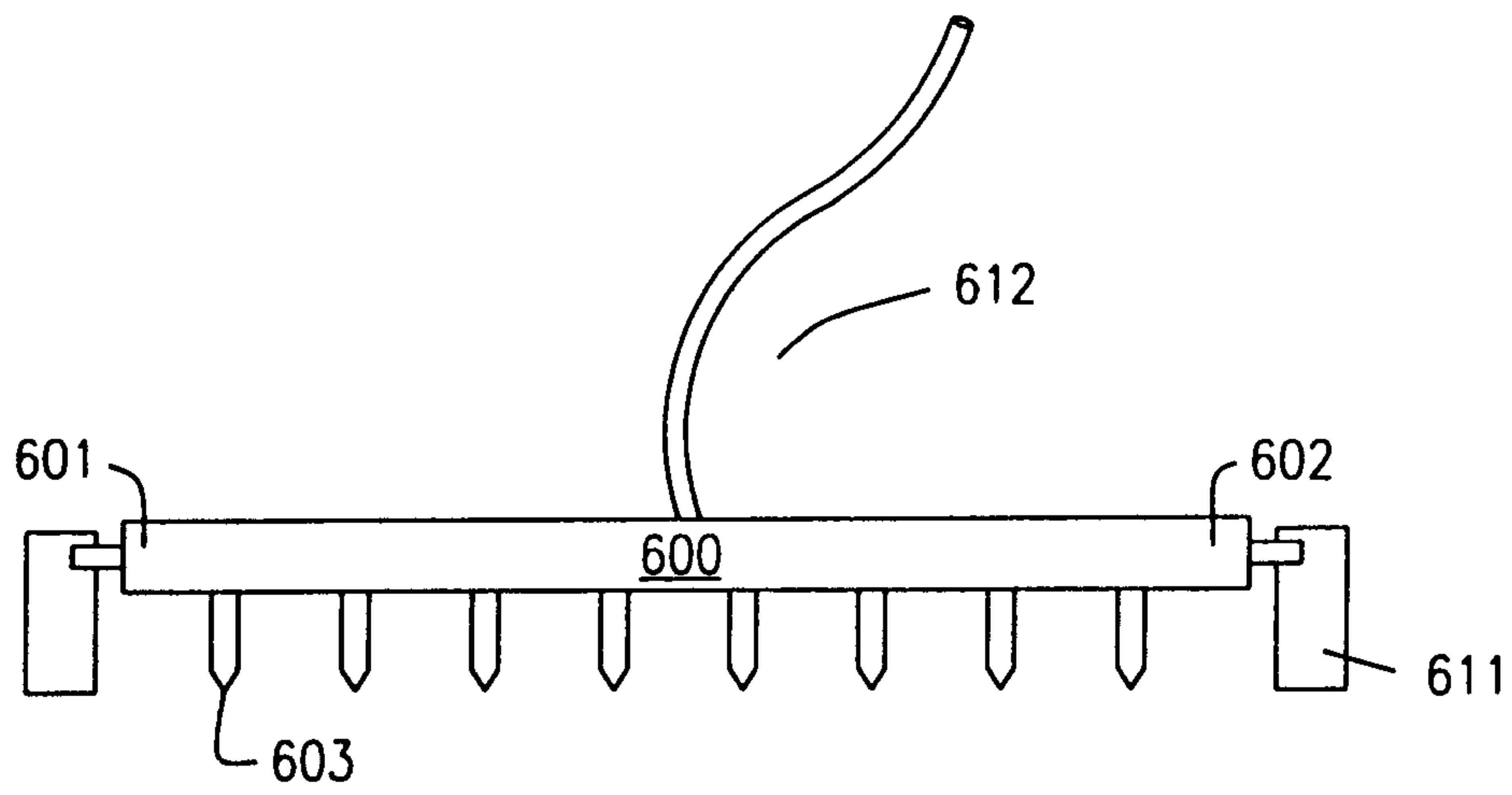


FIG. 48

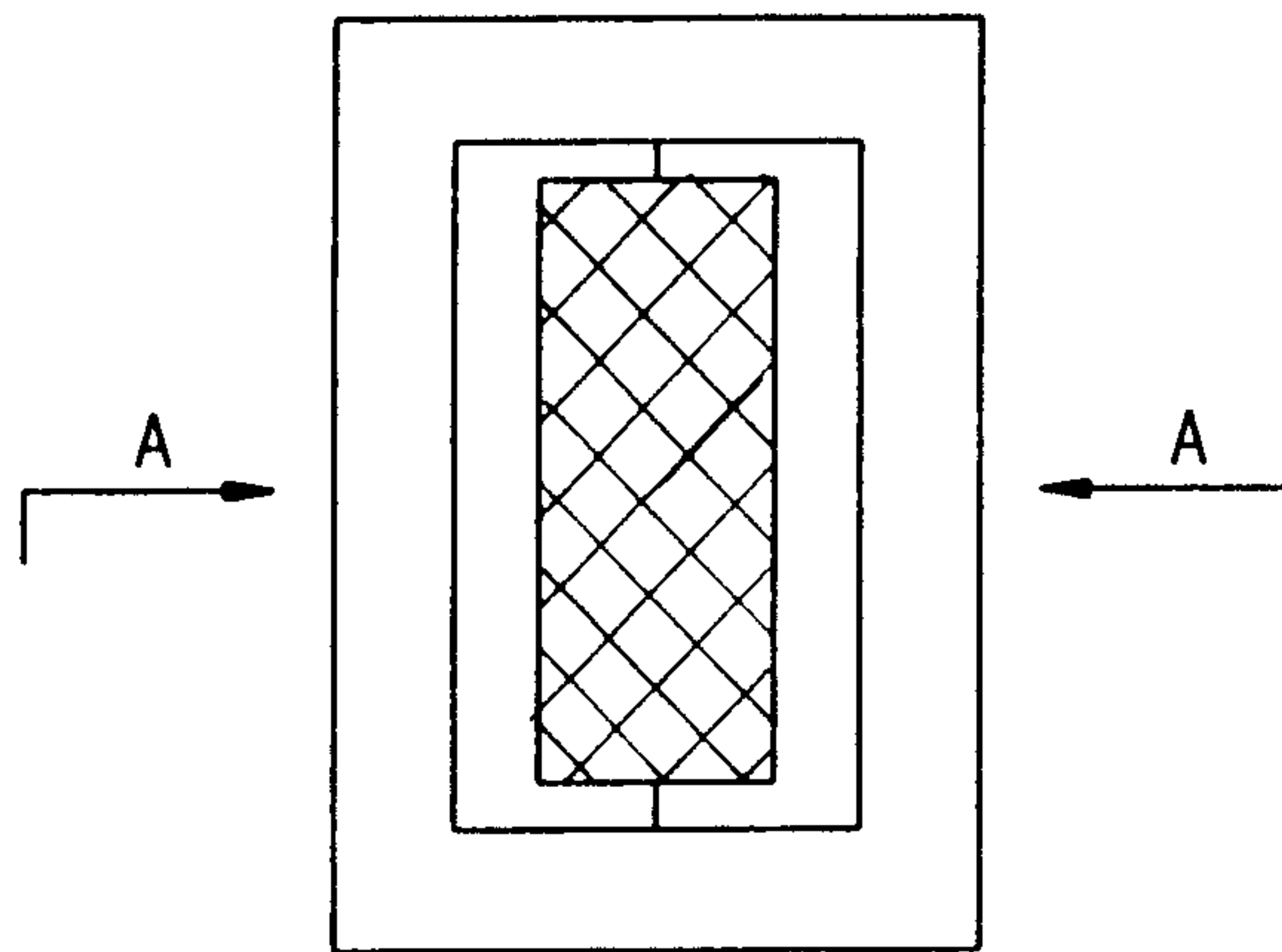


FIG. 49

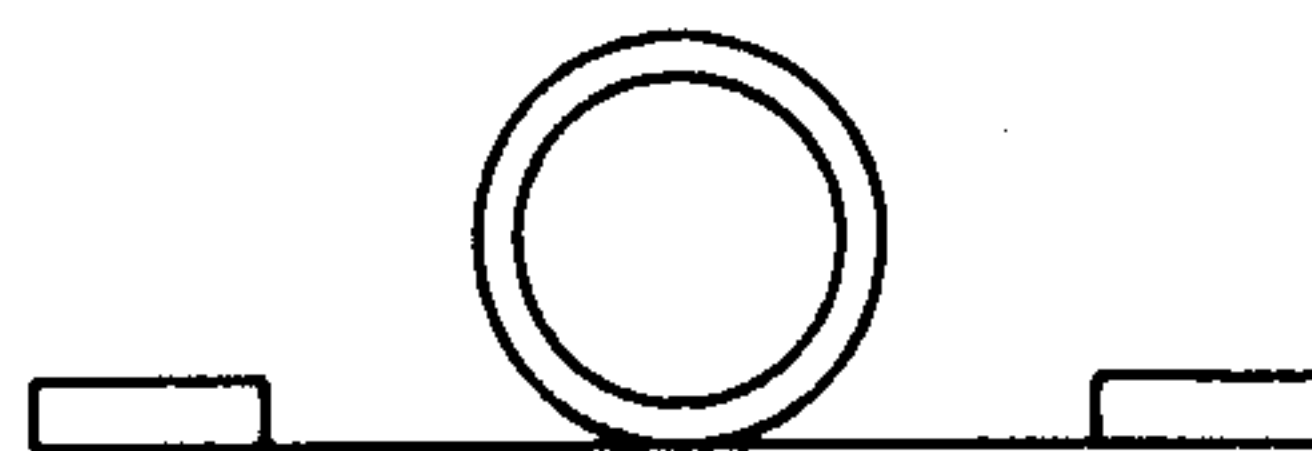


FIG. 50

