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**WO-A1-2008/035089**  
**DE-A1- 19 924 676**  
**US-A1- 2004 243 148**  
**US-A1- 2010 100 011**  
**US-A1- 2010 204 802**  
**US-B1- 6 706 071**  
**US-B2- 8 029 566**  
**EBRAHIM, A. F. ET AL.: 'The use of fiber Bragg grating sensors in biomechanics and rehabilitation applications: The state-of-the-art and ongoing research topics' SENSORS vol. 12, no. 10, 2012, pages 12890 - 12926, XP055280460**  
**GRAICHEN, F. ET AL.: 'Hip endoprosthesis for in vivo measurement of joint force and temperature' JOURNAL OF BIOMECHANICS vol. 32, no. 10, 1999, pages 1113 - 1117, XP008128456**

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# DESCRIPTION

## FIELD OF THE INVENTION

**[0001]** The present invention relates generally to hip replacements, and more specifically, to devices and methods for monitoring the performance of total and partial hip replacements.

## BACKGROUND

### Description of the Related Art

**[0002]** Hip replacement is one of the most common orthopedic surgical procedures. It may be carried out when the patient loses sufficient use of the hip, typically due to injury, avascular necrosis of the hip, or for the treatment of extreme and / or constant joint pain (e.g., due to various types of arthritis (such as rheumatoid or osteoarthritis)).

**[0003]** Hip replacement can take a variety of different forms. In total hip replacement (THR), both the femoral head and the acetabulum are replaced. In a hemi (partial) hip arthroplasty, only the femoral head is replaced while the patient's own acetabulum is retained. The femoral component of a hip replacement may be a single piece with the head and stem as an integral, complete unit, or it may be constructed in several pieces, such as a femoral stem which is then coupled to a separate femoral head piece and neck section (which is often done to provide the patient with custom fitting for length and/or femoral head size). The femoral component can be cemented in place with a bone cement (cemented hip) or it can be fitted precisely within the medullary canal of the femur and held in place without cement (AML - anatomic medullary locking - stem design). Similarly, the acetabular component of a THR can also be a single piece coupled to the hip socket to receives the femoral head, or be a two-piece component with a shell coupled to the pelvic bone and an inner liner attached to the shell. The acetabular component of a THR can be held in place with screws and/or cement or it can be affixed without cement.

**[0004]** Currently, the various components may be made of the same material (e.g., all portions can be made of metal), or individual components can be made from a variety of different materials. For example, it is common for the acetabular component to have a metal shell with an outer surface coating to facilitate bone attachment and ingrowth, and an inner lining made from polyethylene, ultrahigh molecular weight polyethylene, ceramic, or surgical-grade stainless steel. Similarly, there may be several different combinations of materials used in the construction of the femoral head. For example, the femoral head can be composed of metal, usually cobalt chromium (but also stainless steel or titanium), or a ceramic material, while the femoral stem is typically metal (stainless steel, titanium, or cobalt chromium) and often

possesses a surface coating to encourage incorporation of the implant within the femur.

**[0005]** Figure 1 shows a total hip joint of a type known in the art. Figure 2 is an exploded view of the total hip joint of Figure 1. The acetabular shell may be made of any suitable material, preferably a metal or ceramic, and the inner liner may also be made of any suitable material that is compatible with the material for the acetabular shell. For example, the liner may be made of a polyethylene, an ultrahigh molecular weight polyethylene, a ceramic, a metal, or other types of material. The femoral head may be made of a metal or a ceramic and can be of the same, or different, material from that which composes the acetabular liner; for example, a ceramic femoral head on a ceramic acetabular liner (ceramic-on-ceramic hip; COC), a metal femoral head on a metal acetabulum (metal-on-metal hip; MOM) or alternatively a metal or ceramic femoral head on a polyethylene acetabular liner (metal-on-polyurethane, MOP; metal-on-cross-linked-polyurethane, MOXP; ceramic-on-polyurethane, COP; ceramic-on-cross-linked-polyurethane, COXP), or other combinations of the like. The femoral stem is usually made of a metal (stainless steel, titanium, cobalt chromium) that is biocompatible for long-term use in the patient and is inserted into the shaft of the femur and held in place with, or without, bone cement.

**[0006]** Unfortunately, when a total hip is inserted, various complications may arise over time. For example, as shown in Figure 3, there may be wear between the femoral head and the acetabular liner, which leads to improper operation of the artificial hip joint. In addition, the patient may experience inflammation and pain if there is slight movement or dislocation of any of the components. Depending on the types of materials used for the acetabular liner (if present, as in THR) and the femoral head (both THR and Hemi-arthroplasty), there may be wear in the acetabular liner and/or the femoral head which results in loosening or partial (or full) dislocation of the joint, may degrade the performance of the hip, result in difficulty in movement and ambulation, and may cause pain and inflammation for the patient. A second common complication occurs when, over a period of time (for example 8-12 years), bone loss occurs in the tissues surrounding the implant in either the pelvis and/or the femur due to a process known as osteolysis.

**[0007]** Erosion of the bone around the implant may be caused by material debris (metal, ceramic, and/or polyurethane fragments) generated by friction between the femoral head and acetabular cup entering the tissues surrounding the implant and causing inflammation and bone loss. Other potential causes of inflammation and osteolysis are implant vibration and motion, mechanical wear and tear, lack of biocompatibility between the implant materials and the surrounding bone, metal allergy, and lack of biocompatibility between the bone cement and the surrounding bone. Additional complications include infection, nerve damage, material sensitivity, nerve impingement, and hip dislocation (more likely to occur if the muscle has not sufficiently healed; usually during the first 4-12 weeks post-surgery).

**[0008]** Currently, post-operative, in-hospital monitoring of hip replacement surgery patients is conducted through personal visits by the hospital staff and medical team, physical examination of the patient, medical monitoring (vital signs, etc.), evaluation of hip range of motion (ROM),

physiotherapy (including early mobilization and activity), and diagnostic imaging studies and blood work as required. Once the patient is discharged from hospital, prosthesis performance and patient satisfaction is checked during periodic doctor's office visits where a thorough history, physical exam and supplemental imaging and diagnostic studies are used to monitor patient progress and identify the development of any potential complications. During such visits, the surgeon typically evaluates the range of motion of the hip, attempts to identify any pain that occurs during certain motions or actions, and questions the patient to determine activity levels, daily functioning, pain control, and rehabilitation progress.

**[0009]** Unfortunately, most of the patient's recuperative period occurs between hospital or office visits. It can, therefore, be very difficult to accurately measure and follow full joint range of motion (ROM can change depending on pain control, degree of anti-inflammatory medication, time of day, recent activities, and/or how the patient is feeling at the time of the examination), "real life" prosthesis performance, patient activity levels, exercise tolerance, and the effectiveness of rehabilitation efforts (physiotherapy, medications, etc.) from the day of surgery through to full recovery. For much of this information, the physician is dependent upon patient self-reporting or third party observation to obtain insight into post-operative treatment effectiveness and recovery and rehabilitation progress; in many cases this is further complicated by a patient who is uncertain what to look for, has no knowledge of what "normal/expected" post-operative recovery should be, is non-compliant, or is unable to effectively communicate their symptoms. Furthermore, identifying and tracking complications (in and out of hospital) prior to them becoming symptomatic, arising between doctor visits, or those whose presence is difficult to detect would also provide beneficial, additional information to the management of THR patients. Currently, in all instances, neither the physician nor the patient has access to the type of "real time," continuous, objective, prosthesis performance measurements that they might otherwise like to have.

**[0010]** US 2004/243148 A1 discloses miniature sensing devices for use in surgical procedures and devices. A hip replacement prosthesis having sensors coupled thereto is disclosed. WO 2008/035089 A1 discloses "smart implants" that comprise sensors and communication means. US 2010/100011 A1 discloses a system for orthopedic alignment and measurement comprising one or more position sensors, one or more measurement sensors, a processing unit, and a screen. DE 19924676 A1 discloses an artificial hip joint. The present invention discloses novel total and partial hip replacements which overcome many of the difficulties of previous hip prostheses, methods for constructing and monitoring these novel hip replacements, and further provides other related advantages.

## SUMMARY

**[0011]** The invention is defined in the claims. Any subject-matter that is disclosed herein, but which is not defined in the claims does not form part of the invention. Briefly stated, full and partial hip prostheses are provided with a number of sensors to monitor the integrity and efficaciousness of the artificial hip joint within the patient. The sensors may be positioned on

the outer surface of the prosthetic hip, on the inner surfaces of the prosthetic hip, within the prosthetic material (stainless steel, titanium, cobalt chromium, polyurethane, high molecular weight polyurethane, ceramics, etc.) itself, between the various components that comprise the prosthetic hip, within the bone cement (e.g., PMMA, or PMMA and MMA copolymer blends) used to secure the hip (if present), and/or within the tissues surrounding the prosthesis. Within certain embodiments, the sensors are of the type that are passive and thus do not require their own power supply.

**[0012]** Within one aspect of the invention assemblies are provided for positioning and placement within a patient an implant comprising a total or partial hip prosthesis; and a sensor positioned on, in, or around the prosthesis. Within various embodiments the sensor can be positioned on an outer surface of the prosthetic hip, on an inner surface of the prosthetic hip, within the materials used to construct the prosthetic hip, between the various components that make up the prosthetic hip, on or in the bone cement used to secure the prosthetic hip, on or in the tissues surrounding the prosthetic hip (typically bone or bone marrow, but also muscle, ligament, tendon, joint capsule and/or synovial compartment), or any combination of these. Sensors suitable for use within the present invention are accelerometers (acceleration, tilt, vibration, shock and rotation sensors), and optionally pressure sensors, contact sensors, position sensors, chemical microsensors, tissue metabolic sensors, mechanical stress sensors or temperature sensors. Within particularly preferred embodiments the sensor is a wireless sensor, or a sensor connected to a wireless microprocessor.

**[0013]** Within further embodiments a plurality of the aforementioned sensors are positioned on, within, or around (bone cement or tissue) the prosthetic hip, and within preferred embodiments, the prosthetic hip can contain accelerometers and more than one type of sensor (e.g., one or more of, or any combination of the following: tilt sensors, vibration sensors, shock sensors, rotation sensors, pressure sensors, contact sensors, position sensors, chemical microsensors, tissue metabolic sensors, and mechanical stress sensors).

**[0014]** According to various embodiments, sensors are placed at different locations in a replacement hip joint in order to monitor the operation, movement, function, wear, performance, potential side effects and medical status of the artificial hip and its interface with the live tissue of the patient. Live, continuous, *in situ*, monitoring of patient activity, patient function, prosthesis activity, prosthesis function, prosthesis performance, and potential side effects is provided. In addition, information is available on many aspects of the hip replacement prosthesis and its interaction with the patient's own body tissues, including clinically important measurements not currently available through physical examination, medical imaging and diagnostic medical studies.

**[0015]** According to one embodiment the sensors provide evaluation data on the range of motion (ROM) of the hip. Currently, ROM is usually measured clinically by the physician passively moving the hip joint through a full range of motion during physical examination and recording the results (degrees of flexion, extension, abduction, adduction, external rotation, internal rotation and rotation in flexion). Motion sensors and accelerometers can be used to

accurately determine the full ROM of the prosthetic hip joint both during physical examination and during normal daily activities between visits.

**[0016]** According to one embodiment, contact sensors are provided between the prosthesis and the surrounding bone, between the prosthesis and the surrounding bone cement, and/or between the bone cement and the surrounding bone in order to measure bone erosion and loosening around the implant. In other embodiments, strain gauges are provided to detect the strain between the prosthesis and the surrounding bone, between the prosthesis and the surrounding bone cement, between the bone cement and the surrounding bone, and also the strain which is exerted on the various portions of the prosthesis. Sudden increases in strain may indicate that too much stress is being placed on the replacement prosthesis, which may increase damage to the body. For example, a gradual, long-term decrease in strain may cause bone reabsorption around the implant, leading to loosening of the prosthesis or fractures in the bone surrounding the prosthesis.

**[0017]** Accelerometers are provided which detect vibration, shock, tilt and rotation. According to other embodiments, further sensors for measuring surface wear, such as contact or pressure sensors, may be embedded at different depths within the femoral head, the acetabulum, and/or the acetabular cup in order to monitor articular surface erosion. In other embodiments, position sensors, as well as other types of sensors, are further provided which indicate the range of motion and monitor for partial (or complete) hip dislocation in actual use over a period of time.

**[0018]** Within aspects of the disclosure, the artificial hip (total or partial) can contain sensors at specified densities in specific locations. For example, the artificial hip can have a density of sensors of greater than one, two, three, four, five, six, seven, eight, nine, or ten sensors (e.g., acceleration sensors, tilt sensors, vibration sensors, shock sensors, rotation sensors, pressure sensors, contact sensors, position sensors, chemical microsensors, tissue metabolic sensors, and mechanical stress sensors, or any combination of these) per square centimeter of the device. Within other aspects, the artificial hip (total or partial) can have a density of sensors of greater than one, two, three, four, five, six, seven, eight, nine, or ten sensors (e.g., acceleration sensors, tilt sensors, vibration sensors, shock sensors, rotation sensors, pressure sensors, contact sensors, position sensors, chemical microsensors, tissue metabolic sensors, and mechanical stress sensors, or any combination of these) per cubic centimeter of the device. Within related embodiments, the sensors (e.g., acceleration sensors, tilt sensors, vibration sensors, shock sensors, rotation sensors, pressure sensors, contact sensors, position sensors, chemical microsensors, tissue metabolic sensors, and mechanical stress sensors) can be positioned at particular locations on, within, or around the artificial hip, including for example, the femoral stem, the femoral neck, the femoral head, the acetabular cup, the acetabular lining, within portions of the device which are to be connected (e.g., the connecting segments of the femoral stem, femoral neck and femoral head; the connecting segments of the acetabular cup and the acetabular lining), and around the artificial hip (on or in the bone cement used to secure the prosthetic hip, on or in the tissues surrounding the prosthetic hip - typically bone or bone marrow, but also muscle, ligament, tendon, joint capsule and/or synovial

compartment).

**[0019]** Within certain aspects of the disclosure, the total or partial hip prosthesis is provided with a specific unique identifying number, and within further aspects, each of the sensors on, in or around the prosthetic hip each have either a specific unique identification number, or a group identification number (e.g., an identification number that identifies the sensor as an acceleration sensor, a tilt sensor, a vibration sensor, a shock sensor, a rotation sensor, a pressure sensor, a contact sensor, a position sensor, a chemical microsensor, a tissue metabolic sensor, or a mechanical stress sensor). Within yet further aspects, the specific unique identification number or group identification number is specifically associated with a position on, in or around the prosthetic hip.

**[0020]** Within other aspects of the disclosure methods are provided for monitoring an implanted total or partial hip prosthesis comprising the steps of transmitting a wireless electrical signal from a location outside the body to a location inside the body; receiving the signal at a sensor positioned on, in or around an artificial hip located inside the body; powering the sensor using the received signal; sensing data at the sensor; and outputting the sensed data from the sensor to a receiving unit located outside of the body.

**[0021]** The integrity of the partial or total hip prosthesis can be wirelessly interrogated and the results reported on a regular basis. This permits the health of the patient to be checked on a regular basis or at any time as desired by the patient and/or physician.

**[0022]** Within further aspects, each of the sensors contains a signal-receiving circuit and a signal output circuit. The signal-receiving circuit receives an interrogation signal that includes both power and data collection request components. Using the power from the interrogation signal, the sensor powers up the parts of the circuitry needed to conduct the sensing, carries out the sensing, and then outputs the data to the interrogation module. The interrogation module acts under control of a control unit which contains the appropriate I/O circuitry, memory, a controller in the form of a microprocessor, and other circuitry in order to drive the interrogation module. Within yet other aspects the sensor (e.g., an acceleration sensor, a tilt sensor, a vibration sensor, a shock sensor, a rotation sensor, a pressure sensor, a contact sensor, a position sensor, a chemical microsensor, a tissue metabolic sensor, or a mechanical stress sensor) are constructed such that they may readily be incorporated into or otherwise mechanically attached to the hip prosthesis (e.g., by way of a an opening or other appendage that provides permanent attachment of the sensor to the hip prosthesis) and/or readily incorporated into the bone cement or the tissues that surround the hip prosthesis.

**[0023]** Within yet other aspects of the invention methods devices are provided suitable for transmitting a wireless electrical signal from a location outside the body to a location inside the body; receiving the signal at one of the aforementioned sensors positioned on, in or around a prosthetic hip located inside the body; powering the sensor using the received signal; sensing data at the sensor; and outputting the sensed data from the sensor to a receiving unit located outside of the body. Within certain embodiments the receiving unit can provide an analysis of

the signal provided by the sensor.

**[0024]** The data collected by the sensors can be stored in a memory located within the femoral stem. During a visit to the physician, the data can be downloaded via a wireless sensor, and the doctor is able to obtain data representative of real-time performance of the prosthesis.

**[0025]** The advantages obtained include more accurate monitoring of the prosthesis and permitting medical reporting of accurate, *in situ*, data that will contribute to the health of the patient. The details of one or more embodiments are set forth in the description below. Other features, objects and advantages will be apparent from the description, the drawings, and the claims.

#### BRIEF DESCRIPTION OF THE DRAWINGS

**[0026]**

Figure 1 is an isometric view of a total hip replacement.

Figure 2 is an exploded view of the total hip replacement of Figure 1.

Figure 3 shows the total hip replacement within the pelvis of a patient.

Figure 4 is an exploded view of a total hip having sensors thereon according to various embodiments as described herein.

Figure 5 illustrates the embodiment of Figure 4 after the hip has been replaced showing contact locations with the bones of the patient.

Figure 6A is an exploded view of the acetabular cup, a liner, and the femoral having various sensors thereon according to the various embodiments described herein. Figure 6B is an illustration of the incorporation of strain gauges in a variety of locations.

Figure 7A is a side view of the femoral implant with the ball attached.

Figure 7B is an enlarged side view of the femoral implant with various sensors and a power generation segment.

Figure 8A is a top side view of an acetabular cup having various sensors according to the embodiments described herein.

Figure 8B is a liner in the acetabular cup of Figure 9 having various sensors therein.

Figure 9 is a side view of a total assembled hip with examples of different sensor locations.

Figure 10 shows the completed hip assembly of Figure 9 fully functional in a patient, with the various different types of sensors.

Figures 11A and 11B illustrate different types of hip movement which may be measured and monitored according to various embodiments as disclosed herein.

Figure 12 illustrates an information and communication technology system embodiment arranged to process sensor data.

Figure 13 is a block diagram of a sensor, interrogation module, and a control unit according to one embodiment of the disclosure.

Figure 14 is a schematic illustration of one or more sensors positioned on a hip replacement within a subject which is being probed for data and outputting data, according to one embodiment of the disclosure.

#### DETAILED DESCRIPTION OF THE INVENTION

**[0027]** Briefly stated the present invention provides a variety of hip replacements that can be utilized to monitor the integrity and efficaciousness of the device. Prior to setting forth the invention however, it may be helpful to an understanding thereof to first set forth definitions of certain terms that are used hereinafter.

**[0028]** "Hip replacement" as that term is utilized herein, may take a variety of different forms and may involve replacement of all or portions of the patient's hip joint with synthetic materials. In total hip replacement (THR), both the femoral head and the acetabulum are replaced. In a hemi (partial) hip arthroplasty, only the femoral head is replaced while the patient's own acetabulum is retained. The femoral component of a hip replacement may be a single piece with the head and stem as an integral, complete unit, or it may be constructed in several pieces, such as a femoral stem which is then coupled to a separate femoral head piece and neck section (which is often done to provide the patient with custom fitting for length and/or femoral head size). The femoral component can be cemented in place with PMMA bone cement (cemented hip) or it can be fitted precisely within the medullary canal of the femur and held in place without cement (AML - anatomic medullary locking - stem design). Similarly, the acetabular component of a THR can also be a single piece coupled to the hip socket to receive the femoral head, or be a two-piece component with a shell coupled to the pelvic bone and an inner liner attached to the shell. The acetabular component of a THR can be held in place with screws and/or cement or it can be affixed without cement.

**[0029]** Currently, the various components may be made of the same material, for example, all portions can be made of metal, or individual components can be made from a variety of different materials. For example, it is common for the acetabular component to have a metal shell with an outer surface coating to facilitate bone attachment and ingrowth, and an inner lining made from polyethylene, ultrahigh molecular weight polyethylene, ceramic, or surgical-grade stainless steel. Similarly, there may be several different combinations of materials used

in the construction of the femoral head. For example, the femoral head can be composed of metal, usually cobalt chromium (but also stainless steel or titanium), or a ceramic material, while the femoral stem is typically metal (stainless steel, titanium, or cobalt chromium) and often possesses a surface coating to encourage incorporation of the implant within the femur.

**[0030]** As utilized herein the terms "hip implant" or "hip replacement" or "hip replacement or portion thereof" or "medical device" should be understood, unless the specific context requires otherwise, to refer to any or all of the various components that go into making a total hip prosthesis, including for example, the femoral stem, femoral head, and acetabular assembly, as well as their various sub-components. "Hip replacement prosthesis" should be understood to refer to either a partial or total hip replacement prosthesis.

**[0031]** "Sensor" refers to a device that can be utilized to measure one or more different aspects of a body, of a hip implant inserted within a body, and/or the integrity, impact, efficaciousness or effect of the hip implant inserted within a body. Sensors suitable for use within the present invention are accelerometers, and optionally, for example, fluid pressure sensors, contact sensors, position sensors, pulse pressure sensors, blood volume sensors, blood flow sensors, chemistry sensors (e.g., for blood and/or other fluids), metabolic sensors (e.g., for blood and/or other fluids), mechanical stress sensors and temperature sensors. Within certain embodiments the sensor can be a wireless sensor, or, within other embodiments, a sensor connected to a wireless microprocessor. Within further embodiments one or more (including all) of the sensors can have a Unique Sensor Identification number ("USI") which specifically identifies the sensor.

**[0032]** A wide variety of sensors (also referred to as Microelectromechanical Systems or "MEMS", or Nanoelectromechanical Systems or "NEMS", and BioMEMS or BioNEMS, see generally <https://en.wikipedia.org/wiki/MEMS>) can be utilized within the present invention. Representative patents and patent applications include U.S. Patent No. 7,383,071 and U.S. Publication No. 2010/0285082. Representative publications include "Introduction to BioMEMS" by Albert Foch, CRC Press, 2013; "From MEMS to Bio-MEMS and Bio-NEMS: Manufacturing Techniques and Applications" by Marc J. Madou, CRC Press 2011; "Bio-MEMS: Science and Engineering Perspectives" by Simona Badilescu, CRC Press 2011; "Fundamentals of BioMEMS and Medical Microdevices" by Steven S. Saliterman, SPIE-The International Society of Optical Engineering, 2006; "Bio-MEMS: Technologies and Applications", edited by Wanjun Wang and Steven A. Soper, CRC Press, 2012; and "Inertial MEMS: Principles and Practice" by Volker Kempe, Cambridge University Press, 2011; Polla, D. L., et al., "Microdevices in Medicine," Ann. Rev. Biomed. Eng. 2000, 02:551-576; Yun, K. S., et al., "A Surface-Tension Driven Micropump for Low-voltage and Low-Power Operations," J. Microelectromechanical Sys., 11:5, October 2002, 454-461; Yeh, R., et al., "Single Mask, Large Force, and Large Displacement Electrostatic Linear Inchworm Motors," J. Microelectromechanical Sys., 11:4, August 2002, 330-336; and Loh, N. C., et al., "Sub-10 cm<sup>3</sup> Interferometric Accelerometer with Nano-g Resolution," J. Microelectromechanical Sys., 11:3, June 2002, 182-187.

**[0033]** In order to further understand the various aspects of the invention provided herein, the

following sections are provided below: A. Medical Uses of Hip Implants; B. Representative Embodiments of Hip Implants; C. Coatings on Hip Implants; D. Drug-Eluting Hip Implants; E. Methods for Monitoring Infections in Hip Implants; F. Generation of Power; G. Medical Use of Sensors; H. Medical Imaging and Self-Diagnosis of Assemblies Comprising Hip Implants, Predictive Analysis and Predictive Maintenance; I. Methods of Monitoring Assemblies Comprising Hip Implants; and J. Collection, Transmission, Analysis, and Distribution of Data from Assemblies Comprising Hip Implants.

#### **A. MEDICAL USES OF HIP REPLACEMENTS**

**[0034]** Hip replacement is carried out when the patient loses sufficient use of the hip so as to result in disability, loss of movement and function, impaired ambulation, and/or continuous joint pain and discomfort. Common causes of impaired hip function leading to total or partial hip replacement include trauma (typically a hip fracture; often at the femoral neck), avascular necrosis of the hip, or various types of arthritis (such as rheumatoid arthritis or osteoarthritis). In most patients, the operation is successful in improving ambulation, restoring function and reducing pain; as a result, it is one of the most common orthopedic procedures in the Western World.

#### **B. REPRESENTATIVE EMBODIMENTS OF HIP IMPLANTS**

**[0035]** Figure 4 illustrates a prosthesis 10 in the form of a replacement hip having one or more sensors 22 as described herein. The replacement hip includes an acetabular shell 12 in which an acetabular liner 14 is placed. It also includes a femoral assembly 16 which includes two components, a femoral head 18 and a femoral implant or femoral stem 20 (also having a femoral neck 17).

**[0036]** Figure 5 shows the hip replacement prosthesis 10 as positioned in a patient, in an exploded view. As shown in Figure 5, the acetabular shell 12 is fixed to the pelvis bone 23. The femoral stem 20 is coupled to the femur 24 and the femoral head 18 is shown ready for positioning on the femoral stem 20 and also for entering the liner 14 of the acetabular shell. Figures 4 and 5 will be described jointly in order to illustrate various embodiments.

**[0037]** A plurality of sensors 22 are positioned in the prosthesis 10 in order to monitor, *in situ*, the real-time operation of the patient activity and the prosthesis performance. A variety of these sensors will now be described according to various embodiments.

**[0038]** In one embodiment, contact sensors 22 are provided on the outer surface of the acetabular shell 12. These sensors 22 detect and record contact between adjacent parts, such as the between the acetabular shell 12 and the pelvis 23 and/or between the acetabular shell and the bone cement (if present) and/or between the bone cement (if present) and the pelvis.

The contact sensors 22 can detect loosening of the prosthesis 10 and its connection to the surrounding cement (if present) and/or pelvic bone. Loosening of the acetabulum is a common complication that occurs (typically over 8-12 years) when bone loss takes place in the pelvic bones surrounding the acetabulum (e.g., due to a process known as osteolysis). Erosion of the bone around the implant may be caused by material debris (metal, ceramic, and/or polyurethane fragments) generated by friction between the femoral head and acetabular cup entering the pelvic tissues surrounding the acetabulum and causing inflammation and bone loss. Other potential causes of inflammation and osteolysis are implant vibration and motion, mechanical wear and tear, lack of biocompatibility between the implant materials and the surrounding bone, metal allergy, and lack of biocompatibility between the bone cement and the surrounding bone. In addition, the contact sensors 22 may indicate that the acetabular shell 12 is positioned further from the pelvic bone 23 than desired as a result of material debris being built up over time and/or the presence of inflammation between the shell and the pelvic bone. A plurality of contact sensors 22 are positioned at different locations around the acetabular shell 12. In the example shown, a number of sensors are shown positioned on the outer surface of the acetabular shell 12. In various embodiments, these sensors may be positioned in a variety of different patterns based on the contact locations to the pelvis bone and/or the surrounding bone cement (if present). For example, they may be arranged in the pattern of an X, as oval or concentric rings around the acetabular shell from the outermost circumference to the crown or in various other patterns, in order to collect accurate data on the physical contact between the acetabular shell 12 and the pelvic bone 23 and/or surrounding bone cement (if present). Contact sensors can also be dispersed within/arranged within the bone cement (if present) so as to collect data on the physical contact between the bone cement and the acetabular prosthesis and/or between the bone cement and the pelvic bone. Within various embodiments,

**[0039]** Contact sensors 22 may also be positioned at various locations on the two surfaces of the acetabular liner 14. The contact sensors 22 can therefore sense the contact (and/or movement) between the acetabular liner and the acetabular shell (these sensors could be "paired" so as to detect shifting between the acetabular liner and shell), as well as contact between the femoral head and the acetabular liner. Similarly contact sensors 22 can be positioned at various locations on the femoral head to detect contact between the femoral head and the acetabular liner. Thus, in the embodiment of Figures 4 and 5, a variety of contact sensors are provided in order to monitor contact between the bone and the acetabular component, and between the femoral head and the acetabular liner. Dislocation of the femoral head from the natural or synthetic acetabulum of a prosthetic hip is a common complication of hip replacement occurring shortly after surgery (particularly while the surrounding supportive tissues are healing from surgery); sensors on the femoral head and/or acetabulum can alert the patient and the healthcare provider if joint dislocation has occurred. Partial or incomplete dislocation (subluxation) of the hip joint can also occur and may not be readily evident to the patient or the physician; contact sensors on the femoral head and/or acetabulum can determine if the joint is functioning (tracking) correctly and if subluxation (even if subclinical or asymptomatic) is occurring.

**[0040]** Additional contact sensors can be positioned on the femoral stem as well, to monitor contact between the femoral stem and the femur and/or contact between the femoral stem and the surrounding bone cement (if present). Contact sensors can also be dispersed within/arranged within the bone cement (e.g., 22B, if present) so as to collect data on the physical contact between the bone cement and the femoral prosthesis and/or between the bone cement and the femoral canal. These sensors 22 and 22B can detect and record contact between connecting parts in a modular femoral prosthesis, such as the between the femoral head 18, femoral neck 17 and / or the femoral stem 20. These sensors, which can be arranged in corresponding pairs on adjacent pieces, can be used to insure that the connecting elements of a modular femoral prosthesis are properly aligned and fitted. Sensors on the femoral shaft 20 can be used to monitor the contact between the femoral shaft and the femur and/or the contact between femoral shaft and the surrounding bone cement (if present); sensors in the bone cement can be used to monitor the contact between the bone cement (e.g., 22B, if present) and the femur. The contact sensors on the femoral shaft 22 can detect loosening of the prosthesis and its connection to the surrounding cement (if present) and/or the femur. Loosening of the femoral shaft is a common complication that occurs when (typically over 8-12 years), bone loss occurs in the femoral canal surrounding the femoral shaft due to osteolysis. As described above, erosion of the bone around the implant may be caused by material debris (metal, ceramic, and/or polyurethane fragments) generated by friction between the femoral head and acetabular cup entering the femoral tissues surrounding the femoral prosthesis and causing inflammation and bone loss. Other potential causes of inflammation and osteolysis are implant vibration and motion, mechanical wear and tear, lack of biocompatibility between the implant materials and the surrounding bone, metal allergy, and lack of biocompatibility between the bone cement and the surrounding bone. A plurality of contact sensors 22 are positioned at different locations around the femoral shaft. As shown in Figures 4 and 5, sensors are shown positioned on the outer surface of the femoral shaft. In various embodiments, these sensors may be positioned in a variety of different patterns based on the contact locations to the femoral canal and/or the surrounding bone cement (if present). For example, they may be arranged in the pattern of a helix, as vertical lines or concentric rings around the femoral shaft or in various other patterns, in order to collect accurate data on the physical contact between the femoral shaft 20 and the femur and/or surrounding bone cement (if present). Within various aspects of the disclosure contact sensors are placed on the femoral shaft, and the femur and /or bone cement at a density of greater than one, two, three, four, five, six, seven, eight, nine, or ten sensors per square centimeter, or, per cubic centimeter of the device.

**[0041]** Figure 6A illustrates an exploded version of the acetabular shell 12, the liner 14, and the femoral head 18 to permit clear illustration of various positions for strain gauges 26 that can be positioned on the prosthesis. The contact sensors 22 are not shown in Figure 6, but could be used concurrently with the strain gauges and be positioned adjacent to each other or be the same sensor. Strain gauges 26 may be positioned at various locations on the acetabular shell 12 to detect strain encountered between the prosthesis and the surrounding bone. A decrease in strain may indicate that there is bone resorption (loss), which could lead to loosening of the prosthesis, or fractures. The strain sensors 26 provide a different data point than the contact sensors 22. The contact sensors 22 merely specify whether there is current

contact between adjacent structures and thus provide a good indication of whether there is abutting contact between two surfaces. However, they do not provide an indication of the strain that is present in either of the surfaces, on the other hand, the strain sensors 26 output data indicative of the mechanical strain forces being applied across the implant which, if not corrected, can be a harbinger of future loosening and prosthesis failure. In addition, the strain gauges 26 may be of the type which indicates the strain which is being exhibited between two surfaces, such as between the acetabular liner and the pelvic bone or between the acetabular shell 12 and the acetabular liner 14. Further, such strain gauges may collect data regarding the strain and location of such strain between the femoral head 18 and the acetabular liner 14.

**[0042]** As shown in Figure 6B, strain gauges can be located on the femoral prosthesis; particularly the femoral stem, but also the femoral neck and the femoral head. Strain gauges may be positioned at various locations on the femoral stem to detect strain encountered between the prosthesis and the surrounding bone. A decrease in strain may indicate that there is bone resorption (loss) in the femoral canal, which could lead to loosening of the prosthesis, or femoral fractures. The strain sensors can provide an indication of the strain that is present in the femoral shaft and measure the most important mechanical strain forces being applied across the implant which, if not corrected, have a high probability of resulting in loosening and prosthesis failure. Within various aspects of the disclosure strain sensors are placed on the acetabular shell, acetabular liner, femoral shaft, and the femur and /or bone cement at a density of greater than one, two, three, four, five, six, seven, eight, nine, or ten sensors per square centimeter, or, per cubic centimeter of the device.

**[0043]** Figures 7A and 7B illustrate one embodiment in which accelerometers are positioned at various locations in and on the femoral shaft 18, femoral neck and femoral head. In particular, as shown in Figure 7A one or more accelerometers may be positioned on the femoral head 16. In addition, one or more acceleration sensors 42 in the form of accelerometers or gyroscopes can be positioned on the surface of or inside the femoral shaft portion 18. Accelerometers provide the benefit of being able to detect acceleration, vibration, shock, tilt, and rotation of various components. They permit the ability to measure performance of the prosthesis 10 under various conditions and over long periods of time. In this particular example, the prosthesis 10 is a hip replacement joint. Of course, it could be any other prosthesis, such as a prosthetic elbow joint, shoulder joint, metacarpal joint, ankle joint, or the like. Within various aspects of the disclosure strain sensors are placed on the acetabular shell, acetabular liner, femoral shaft, and the femur and /or bone cement at a density of greater than one, two, three, four, five, six, seven, eight, nine, or ten sensors per square centimeter, or, per cubic centimeter of the device.

**[0044]** Shortly after the hip has been replaced, the leg will be mobilized, at first passively, then actively; shortly thereafter, the patient will begin gradual weight bearing on the joint. The accelerometers 42 will measure the movement of the hip socket during movement, including during ambulation as the leg swings forward, hits the ground, plants, is lifted off the ground, and the body is propelled forward. In addition, the accelerometers will measure the impact of the foot hitting the ground and the effect of the force being transferred through the femur to the

pelvic bones and any vibration, shock or rotation which may occur at different locations in the prosthesis 10. As the patient continues to improve their range of motion postoperatively, the acceleration experienced at different locations in the prosthetic hip joint, can be monitored. It will be expected that as the patient heals from the surgery, activity levels will progressively increase, ambulation will improve, steps will be more rapid (and fluid) and, in addition, greater stride length will be achieved with each step. This may result in greater impact every time the foot hits the ground, which can be measured over time (and compared to previous values) by the various accelerometers 42 positioned on the femoral head 16, in the femoral stem 18 and in other locations on the prosthesis 10. Postoperative progress can be monitored (readings compared from day-to-day, week-to-week, etc.) and the information compiled and relayed to both the patient and the attending physician allowing rehabilitation to be followed sequentially and compared to expected (typical population) norms. Within certain embodiments, a wearable device interrogates the sensors on a selected or randomized basis, and captures and /or stores the collected sensor data. This data may then be downloaded to another system or device (as described in further detail below).

**[0045]** Integrating the data collected by the sensors described herein (e.g., contact sensors, and/or strain gauges and accelerometers) with simple, widely available, commercial analytical technologies such as pedometers and global positioning satellite (GPS) capability, allows further clinically important data to be collected such as, but not restricted to: extent of patient ambulation (time, distance, steps, speed, cadence), patient activity levels (frequency of activity, duration, intensity), exercise tolerance (work, calories, power, training effect), range of motion (discussed later) and prosthesis performance under various "real world" conditions. It is difficult to overstate the value of this information in enabling better management of the patient's recovery. An attending physician (or physiotherapist, rehabilitation specialist) only observes the patient episodically during scheduled visits; the degree of patient function at the exact moment of examination can be impacted by a multitude of disparate factors such as: the presence or absence of pain, the presence or absence of inflammation, stiffness, time of day, compliance and timing of medication use (pain medications, anti-inflammatories), recent activity and exercise levels, patient strength, mental status, language barriers, the nature of their doctor-patient relationship, or even the patient's ability to accurately articulate their symptoms - to name just a few. Continuous monitoring and data collection can allow the patient and the physician to monitor progress objectively by supplying information about patient function under numerous conditions and circumstances, to evaluate how performance has been affected by various interventions (pain control, exercise, physiotherapy, anti-inflammatory medication, rest, etc.), and to compare rehabilitation progress versus previous function and future expected function. Better therapeutic decisions and better patient compliance can be expected when both the doctor and the patient have the benefit of observing the impact of various treatment modalities on patient rehabilitation, activity, function and overall performance.

**[0046]** The sensor used for the contact, strain and accelerometers can be an acceptable type of those generally available (see e.g., U.S. Patents 7,450,332; 7,463,997 and 7,924,267 which describe various types of such sensors, including MEMs sensors that can act as strain gauges, accelerometers and many other sensing functions). The particular sensor described in U.S.

patent 7,450,332, which detects free fall of an object and motion of an object with respect to a gravity field, would have particular benefits in being able to detect and store all the forces acting on the leg and the full motion of the leg, during passive and active motion and when it is swinging in between steps, both before, after and during impact with the ground.

**[0047]** Figures 7A, 8A and 8B illustrate yet another type of sensor, articular surface wear sensors 46 that may be positioned at various locations in the acetabular liner and the femoral head. According to one embodiment, one or more articular surface wear sensors are positioned at various depths of the acetabular liner 14 as shown in Figures 7A and 8B and/or the femoral head 16. These sensors 46 for measuring the surface wear may be contact pressure sensors that are embedded within the acetabular liner and/or femoral head at varying depths in order to monitor articular surface erosion (and provide data as to the extent and depth of surface wear of the two components). They may also be positioned between the acetabular shell 12 and the acetabular liner 14 as shown in Figures 8A and 8B in order to monitor any kind of wear or degradation of the physical contact between the shell 12 and the liner 14.

**[0048]** Figure 9 shows an example of the complete prosthesis in the form of a hip replacement prosthesis having a plurality of different sensors (e.g., 22, 24, 42, 44, and 46) thereon. It may include, in a single prosthesis hip 10, a plurality of contact sensors 22, strain gauges 24, accelerometers 42, articular wear surface sensors 46, as well as electric power generation structure 44. In addition, a plurality of position sensors can also be placed to monitor, record and transfer the exact position of the head 18 relative to the acetabular liner 14.

**[0049]** Figure 10 illustrates different locations at which position sensors 52 and/or accelerometers 53 may be located in the prosthesis. The position sensors 52, as well as accelerometers 53, can be contained within the femoral stem or within the neck, or within the femoral head, both proximally and distally. They can also be contained within the acetabular component, both the liner and the shell. By placing position sensors and/or accelerometers along the length of the femoral stem, the exact location of the femur as compared to the acetabular component and to the pelvis can be exactly determined and stored in memory. Similarly, by placing accelerometers at different locations in the neck and the head of the femoral implant, the amount of pressure applied at different locations, the movement at the locations and the relative positions of the components to each other can be exactly determined. Similarly, such sensors enhance the accuracy of a physical exam and provide for the ability to detect full dislocation or partial dislocation (subluxation) of the hip joint.

### **C. COATINGS ON HIP IMPLANTS**

**[0050]** Within certain aspects of the disclosure the hip implants are provided that can have one or more coatings on one or more surfaces of the hip implant. Coatings can be provided on hip implant for a variety of purposes. Coatings may be biodegradable, or non-biodegradable, or a combination of these. Representative examples of coatings are polymer-based (e.g., polymers

comprised of polyurethane, polyester, polylactic acid, polyamino acid, polytetrafluoroethylene, teflon, Gortex®), although non-polymer coatings may also be utilized. Within certain embodiments of the disclosure, one or more sensors as described herein may be disbursed throughout the coating (e.g., even in a random manner).

#### **D. DRUG -ELUTING HIP IMPLANTS**

**[0051]** Within certain aspects of the disclosure drug-eluting hip implants are provided which comprise one or more sensors, and which can be utilized to release a desired agent (e.g., a drug or therapeutic agent) to a desired location within the body. Representative examples of suitable anti-scarring or anti-fibrotic drugs include disclosed in US Patent. No. 5,716,981; US Patent App. Nos. 2005/0021126 and 2005/0171594; and US Patent App. Nos. 2005/0181005 and 2005/0181009.

**[0052]** A drug-eluting delivery device may be included within the hip implant in order to release a desired drug upon demand (e.g., upon remote activation / demand, or based upon a timed schedule, see generally U.S. Patent App. No. 2011/0092948 entitled "Remotely Activated Piezoelectric Pump For Delivery of Biological Agents to the Intervertebral Disc and Spine"), or upon detection of an activating event (e.g., detection of a leak by a pressure sensor). For example, within certain aspects of the disclosure biological agents can be administered along with or released from a hip implant in order to treat or prevent disease (e.g., i) in the case of cancer with a chemotherapeutic agent, or in the case of preventing restenosis, or ii) in the case of infection, with an antimicrobial drug).

**[0053]** Within preferred aspects of the disclosure one or more sensors (e.g., pressure sensors, contact sensors, and/or position sensors) can be utilized to determine appropriate placement of the desired drug, as well as the quantity and release kinetics of drug to be released at a desired site.

#### **E. METHODS FOR MONITORING INFECTION**

**[0054]** Within other embodiments hip implants are provided comprising one or more temperature sensors. Such hip implants can be utilized to measure the temperature of the joint, the hip implant, and in the local tissue and environment adjacent to the hip implant. Methods are also provided for monitoring changes in temperature over time, in order to determine and /or provide notice (e.g., to a patient and/or a healthcare provider) that an infection may be imminent.

**[0055]** In certain aspects of the present disclosure, metabolic and physical sensors can be utilized to monitor for rare, but potentially life-threatening complications of joint replacement surgery. In a small number of patients (<1%), the prosthetic joint and surrounding tissues can

become infected; typically from bacteria colonizing the patient's own skin that contaminate the surgical field (often *Staphylococcus aureus* or *Staphylococcus epidermidis*). Sensors such as temperature sensors (detecting temperature increases), pH sensors (detecting pH decreases), and other metabolic sensors can be used to suggest the presence of infection on or around the implant. Early detection of infection could allow preemptive treatment with antibiotics or surgical drainage and eliminate the need to surgically remove the prosthesis.

#### **F. GENERATION OF POWER**

**[0056]** Figure 7B illustrates a particular benefit that can be obtained as the patient ambulates with the new prosthetic hip. As shown in Figure 7B, a small electrical generation unit 44 can be positioned along an outer, or alternatively an inner, surface of the femoral stem 18. In particular, every time a user takes a step, there is a release of pressure and an increase of pressure inside the internal structure of the femoral stem 16. Using the appropriate piezoelectric materials or microelectric generators, a small amount of electricity can be generated with each step that is taken. The electricity can be stored in capacitors also mounted inside the femoral stem 16. The electricity can then be used to power the sensors that are positioned at the various locations inside the prosthesis.

**[0057]** A variety of techniques have been described for scavenging power from small mechanical movements or mechanical vibration. See, for example, the article entitled "Piezoelectric Power Scavenging of Mechanical Vibration Energy," by U.K. Singh et al., as published in the Australian Mining Technology Conference, October 2-4, 2007, pp. 111-118. This paper provides examples of different types of power scavengers which can produce electricity from very small motion and store the electricity for later use. The above article also describes embodiments in which pressure is applied and released from the particular structure in order to produce electricity without the need for motion, but rather as a result of the application of high pressure. As explained in the embodiments herein, force is applied to the internal structure of the femoral stem 16 when the patient puts his weight on the leg during a step and such force can produce more than enough electric power to operate all of the sensors which are described herein. Other mechanisms that can produce electricity from very small amounts of repetitive motion are described U.S. Patent Application Publication No. 2010/0164705, published on July 1, 2010. This patent application describes techniques by which energy can be harvested in the rotation of a tire and then the harvested energy can be used to power a plurality of different sensors and then, at selected time periods, the selected sensors can output the collected data to a central collection site. Other sensors of this type are described in issued U.S. Patent No. 7,603,894, entitled "Self-Powered Tire Monitoring System."

**[0058]** In one preferred embodiment, the electrical generation system is motionless and relies solely on pressure that is applied during the step and the release of that pressure when the step is completed and the leg swings free for the next step. Since there is no motion, the patient will not feel any sensation due to small changes in the position or length of the femoral stem 18 during the step. Rather, the length is kept constant and the electricity is generated by

piezoelectric structures or by internal suspended structures which do not form part of the support structure of the femoral stem 18.

**[0059]** Other techniques may also be utilized to scavenge for power, include, for example, those disclosed in an article entitled "Next Generation Micro-power Systems by Chandrakasan et al., as published in the 2008 Symposium on VLSI Circuits Digest of Technical Papers, pp. 1-5, (see also U.S. Patent No. 8,283,793 entitled "Device for Energy Harvesting within a Vessel," and U.S. Patent No. 8,311,632 entitled "Devices, Methods and Systems for Harvesting Energy in the Body,").

**[0060]** After the electricity is generated by one or more generators 44, the electricity is transmitted to any one of the variety of sensors which is described herein. For example, it can be transmitted to the contact sensors 22, the strain gauges 24, or the accelerometers 42. It may also be transmitted to the other sensors that will be described later herein. The transmission of the power can be carried out by any acceptable technique. For example, if the sensor is physically coupled to the femoral stem electric wires may run from the generator 44 to the particular sensor, for example accelerometers 42 or other surface wear structures that are part of the femoral stem. For those sensors which are in the acetabular component, the electricity can be transmitted wirelessly in the same way that wireless smartcards receive power from closely adjacent power sources using the appropriate send and receive antennas. Such send and receive techniques of electric power are also described in the publication and the patent applications and issued U.S. patent previously described.

#### **G. MEDICAL USE OF SENSORS**

**[0061]** Figures 11A and 11B indicate examples of uses of the sensors during a physical examination of the patient and the different types of data which may be obtained from the sensors which have been implanted according to the teachings herein. The sensors provide evaluation data on the range of motion (ROM) of the hip. Currently, ROM is usually measured clinically by the physician passively moving the hip joint through a full range of motion during physical examination and recording the results (degrees of flexion, extension, abduction, adduction, external rotation, internal rotation and rotation in flexion). Motion sensors and accelerometers can be used to accurately determine the full ROM of the prosthetic hip joint both during physical examination and during normal daily activities between visits. As shown in Figure 11A, one primary factor in the health of the hip is the angle X that the patient is able to achieve at various times during physical therapy as they recover from the surgery. As the angle X becomes smaller and smaller, the doctor can be assured that joint function is improving. By tracking angle X over time the physical therapist can monitor the progress of the patient, assess whether scar tissue formation, subluxation, or other pathology is limiting/affecting ROM of the hip, and change/implement treatment as needed. With the sensors installed as indicated herein, the physical therapist or physician does not need to guess the angle being achieved, rather, if the leg is positioned adjacent to a read out computer, the exact angle can be known at the very moment that the joint is being clinically evaluated. On the other hand, if X does not

continue to decrease, but remains large (or increases), the physical therapist or physician can be alerted to problems which the patient may be having in rehabilitation or delayed recovery from the surgery and can investigate and/or take action sooner rather than later. Similarly, the embodiment of Figure 11B indicates measurements that can be taken when the user holds the leg at exactly a 90° angle Y as shown. With the leg held firmly at 90°, data can be collected from the various sensors throughout the leg in order to determine the strain, the contact locations, acceleration and other data. The position sensors as used herein can alert the patient that the leg is held at exactly 90° so that the collecting of the data can be accurate as data is collected at different times over several months as the patient is monitored. While flexion and extension are illustrated in the sited figures, it should be obvious to one of skill in the art that data can also be collected for abduction, adduction, external rotation, and internal rotation and rotation in flexion of the hip. Additionally, ROM can also be monitored between patient visits by interpreting ROM generated during daily activities when the patient is at home.

**[0062]** Some aspects of the operation and the benefits obtained thereby will now be explained. One particular benefit is the live and in-situ monitoring of the patient's recovery and the hip implant 10. The sensors as described herein are collecting data on a constant basis, during normal daily activities and even during the night if desired. Namely, the strain will be measured, collected and stored on a regular basis over long periods of time with particular measurements being taken at regular intervals. For example, the contact sensors can obtain and report data once every 10 seconds, once a minute, or once a day. Other sensors will collect data more frequently, such as several times a second. For example, it would be expected that the acceleration and position data would be collected and stored several times a second. Other types of data might only need to be collected by the minute or by the hour. Since the femoral stem contains a large internal portion which, in the prior art might be hollow or a solid bar of metal, this internal structure has more than sufficient space in order to house one or more processor circuits, CPUs, memory chips and other electrical circuits as well as antennas for sending and receiving the data. The processors can be programmed to collect data from the various sensors on any desired schedule as set by the medical professional. All activity can be continuously monitored post operation and the data collected and stored in the memory located inside the femoral stem 18.

**[0063]** A patient will generally have regular medical checkups. When the patient goes to the doctor's office for a medical checkup, the doctor will bring a reading device closely adjacent the implant 10, in this example a hip replacement, in order to transfer the data from the internal circuit inside the femoral stem 18 to the database in the physician's office. The use of wireless transmission using smartcards or other techniques is very well known in the art and need not be described in detail. Examples of such wireless transmission of data are provided in the published patent applications and patents which have been described herein. The data which has been collected based on the patient's movement and use of the leg over the prior several weeks or even several months is transferred in a few moments from the memory which is positioned in the femoral stem 18 to the doctor's computer or wireless device. The computer therefore analyzes the data for anomalies, unexpected changes over time, positive or negative trends, and other signs which indicative of the health of the patient and the operability of the

prosthesis. In addition, the physician can collect data that details the record of all impacts to the joint, including the magnitude and the direction of the acceleration. If the physician locates a high acceleration event, such as the patient falling, or other physical activities or exercise, the physician can be alerted to inquire of the patient of any problems they may have had during a fall or, alternatively, warn the patient against too vigorous an activity which may potentially cause damage to the hip implant. For example, if the patient has decided to go skiing or jogging, the doctor will be able to monitor the effect of such activity on the implant 10, including the accelerations and strains during the event itself. The doctor can then look at the health of the prosthesis in the hours and days after the event and compare it to data prior to the event to determine if any particular event caused long term damage, such as a separation of the prosthesis from the surrounding bone tissue or joint subluxation, or if the activities subjected the implant to stress/strain/impact forces beyond the manufacturer's performance specifications for that particular artificial joint. Data can be collected and compared with respect to the ongoing and long term performance of the implant from the strain gauges, the contact sensors, the surface wear sensors, or other sensors which may be present.

**[0064]** In one alternative, the patient may also have such a reading device in their home which collates the data from the implant on a periodic basis, such as once per day or once per week. Empowering the patient to follow their own rehabilitation - and enabling them to see the positive (and negative) effects of various lifestyle choices on their health and rehabilitation - can be expected to improve compliance and improve patient outcomes. Furthermore, their experience can be shared via the web with other patients to compare their progress versus expected "norms" for function and rehabilitation and alert them to signs and symptoms that should be brought to their doctor's attention. The performance of different implants can be compared in different patients (different sexes, weights, activity levels, etc.) to help manufacturers design better prostheses and assist orthopedic surgeons in the selection of the right prosthesis for specific patient types. Payers, patients, manufacturers and physicians could all benefit from the collection of this comparative information. Lastly, data accumulated at home can be collected and transmitted via the Internet to the physician's office for analysis - potentially eliminating unnecessary visits in some cases and encouraging immediate medical follow-up in others.

#### **H. MEDICAL IMAGING AND SELF-DIAGNOSIS OF ASSEMBLIES COMPRISING HIP IMPLANTS; PREDICTIVE ANALYSIS AND PREDICTIVE MAINTENANCE**

**[0065]** The present invention provides hip implants which are capable of imaging through the use of sensors over a wide variety of conditions. For example, within various aspects of the disclosure methods are provided for imaging a hip implant, or an assembly comprising a hip replacement with sensors, comprising the steps of detecting the changes in sensors in, on, and or within a hip implant over time, and wherein the hip implant comprises sensors at a density of greater than 1, 2, 3, 4, 5, 6, 7, 8, 9, 10 or 10 sensors per square centimeter. Within other aspects the hip implant comprises sensors at a density of greater than 1, 2, 3, 4, 5, 6, 7, 8, 9, 10 or 10 sensors per cubic centimeter. Within either of these aspects there can be less than

50, 75, 100, or 100 sensors per square centimeter, or per cubic centimeter. As noted above, a wide variety of sensors can be utilized therein, including for example, contact sensors, strain gauge sensors, pressure sensors, fluid pressure sensors, position sensors, pulse pressure sensors, blood volume sensors, blood flow sensors, blood chemistry sensors, blood metabolic sensors, mechanical stress sensors, and temperature sensors.

**[0066]** For example, a hip implant comprising sensors as described herein can be utilized to image hip anatomy through sensors which can detect positional movement. The sensors used can also include accelerometers and motion sensors to detect movement of the hip implant due to a variety of physical changes. Changes in the position of the accelerometers and/or motion sensors over time can be used as a measurement of changes in the position of the hip implant over time. Such positional changes can be used as a surrogate marker of hip anatomy - i.e. they can form an "image" of the hip implant to provide information on the size, shape and location of changes to the hip implant, and/or hip implant movement/migration. For example, loosening of the hip implant (typically in the femoral stem or acetabular shell) can result in unwanted movement of the prosthesis relative to bone in which it is implanted during activity and weight bearing. By utilizing sensors in the present invention, it is possible to determine the location of the unwanted movement and the degree of movement present during different motions and activities. Similarly, monitoring changes in the joint space (i.e. the change in the space separating the femoral and the acetabular components) over time can be used as an indicator of joint surface (femoral head and/or acetabular liner) erosion and wear. Finally, following the movement of the sensors throughout their range of motion can provide a dynamic "image" of the joint; allowing the clinician to monitor both improvement and decline in joint function (and surrounding tissues) over time.

**[0067]** Certain exemplary embodiments will now be explained in more detail. One particular benefit is the live and in-situ monitoring of the patient's recovery with a hip implant. The sensors as described herein can collect data on a constant basis, during normal daily activities and even during the night if desired. For example, the contact sensors can obtain and report data once every 10 seconds, once a minute, or once a day. Other sensors will collect data more frequently, such as several times a second. For example, it would be expected that the temperature, contact, and /or position data could be collected and stored several times a second. Other types of data might only need to be collected by the minute or by the hour. Still other sensors may collect data only when signaled by the patient to do so (via an external signaling/triggering device) as part of "event recording" - i.e. when the patient experiences a particular event (e.g. pain, injury, etc.) - and signals the device to obtain a reading at that time in order to allow the comparison of subjective/symptomatic data to objective/sensor data in an effort to better understand the underlying cause or triggers of the patient's symptoms.

**[0068]** In certain instances the hip implant is of sufficient size and has more than sufficient space in order to house one or more processor circuits, CPUs, memory chips and other electrical circuits as well as antennas for sending and receiving the data. Within other embodiments, the associated medical device may be able to house the one or more processor circuits, CPUs, memory chips and other electrical circuits as well as antennas for sending and

receiving the data. Processors can be programmed to collect data from the various sensors on any desired schedule as set by the medical professional. All activity can be continuously monitored post operation or post-procedure and the data collected and stored in the memory located inside the hip implant.

**[0069]** A patient with a hip implant will generally have regular medical checkups. When the patient goes to the doctor's office for a medical checkup, the doctor will bring a reading device closely adjacent to the hip implant, in this example the hip implant, in order to transfer the data from the internal circuit inside the hip implant to the database in the physician's office. The use of wireless transmission using smartcards or other techniques is very well known in the art and need not be described in detail. Examples of such wireless transmission of data are provided in the published patent applications and patents which have been described herein. The data which has been collected (e.g., over a short period of time, over several weeks or even several months) is transferred in a few moments from the memory which is positioned in the hip implant to the doctor's computer or wireless device. The computer therefore analyzes the data for anomalies, unexpected changes over time, positive or negative trends, and other signs which may be indicative of the health of the patient and the operability of the hip implant. For example, if the patient has decided to go skiing or jogging, the doctor will be able to monitor the effect of such activity on the hip implant, including changes during such activities. The doctor can then look at the health of the hip implant in the hours and days after the event and compare it to data prior to the event to determine if any particular event caused long term damage, or if the activities subjected the hip implant to forces beyond the manufacturer's performance specifications for that particular hip implant. Data can be collected and compared with respect to the ongoing and long term performance of the hip implant from the strain gauges, the contact sensors, the surface wear sensors, or other sensors which may be present. One representative example of an electronic data capture, documentation and clinical decision support system (EDDS) is provided in WO 2012/061825.

**[0070]** In one alternative, the patient may also have such a reading device in their home which collates the data from the hip implant on a periodic basis, such as once per day or once per week. As described above, the patient may also be able to "trigger" a device reading (via an external signaling/triggering device) as part of "event recording." Empowering the patient to follow their own rehabilitation - and enabling them to see the positive (and negative) effects of various lifestyle choices on their health and rehabilitation - can be expected to improve compliance and improve patient outcomes. Furthermore, their experience can be shared via the web with other patients to compare their progress versus expected "norms" for function and rehabilitation and alert them to signs and symptoms that should be brought to their doctor's attention. The performance of different hip implants can be compared in different patients (different sexes, weights, activity levels, etc.) to help manufacturers design better devices and assist surgeons and other healthcare providers in the selection of the right hip implant for specific patient types. Payers, patients, manufacturers and physicians could all benefit from the collection of this comparative information. Lastly, data accumulated at home can be collected and transmitted via the Internet to the physician's office for analysis - potentially eliminating unnecessary visits in some cases and encouraging immediate medical

follow-up in others.

## I. METHODS OF MONITORING HIP IMPLANTS

**[0071]** As noted above, the present disclosure also provides methods for monitoring one or more of the hip implants provided herein. For example, Figure 12 illustrates a monitoring system usable with the hip implant 10 as of the type shown in any one of Figures described above. The monitoring system includes a sensor (e.g., 22, 22B, 24, 42 and/or 46) an interrogation module 124, and a control unit 126. The sensor (e.g., 22, 22B, 24, 42 and/or 46) is of the passive, wireless type which can operate on power received from a wireless source. Such sensors of this type are well known in the art and widely available. A pressure sensor of this type might be a MEMS pressure sensor, for example, Part No. LPS33 1AP, sold on the open market by STMicroelectronics. MEMS pressure sensors are well known to operate on very low power and suitable to remain unpowered and idle for long periods of time. They can be provided power wirelessly on an RF signal and, based on the power received wirelessly on the RF signal, perform the pressure sensing and then output the sensed data.

**[0072]** In one aspect, an electrical generation system (as described above) is provided that can be utilized to power the sensors described herein. During operation, as shown in Figure 12, an interrogation module 124 outputs a signal 128. The signal 128 is a wireless signal, usually in the RF band, that contains power for the sensor (e.g., 22, 22B, 24, 42 and/or 46) as well as an interrogation request that the sensors 22 perform a sensing. Upon being interrogated with the signal 128, the sensor (e.g., 22, 22B, 24, 42 and/or 46) powers up and stores power in onboard capacitors sufficient to maintain operation during the sensing and data reporting. Such power receiving circuits and storing on onboard capacitors are well known in the art and therefore need not be shown in detail. The appropriate sensing is carried out by the sensor (e.g., 22, 22B, 24, 42 and/or 46) and then the data is output from the sensor back to the interrogation module 124 on a signal 130, where it is received at an input port of the integration module.

**[0073]** According to one aspect, sufficient signal strength is provided in the initial signal 128 to provide power for the sensor and to carry out the sensing operation and output the signal back to the interrogation module 124. In other aspects, two or more signals 128 are sent, each signal providing additional power to the sensor to permit it to complete the sensing operation and then provide sufficient power to transfer the data via the signal path 130 back to the interrogation module 124. For example, the signal 128 can be sent continuously, with a sensing request component at the first part of the signal and then continued providing, either as a steady signal or pulses to provide power to operate the sensor. When the sensor is ready to output the data, it sends a signal alerting the interrogation module 124 that data is coming and the signal 128 can be turned off to avoid interference. Alternatively, the integration signal 128 can be at a first frequency and the output signal 130 at a second frequency separated sufficiently that they do not interfere with each other. In a preferred aspect, they are both the same frequency so that the same antenna on the sensor can receive the signal 128 and send

signal 130.

**[0074]** The interrogation signal 128 may contain data to select specific sensors on the hip replacement. For example, the signal 128 may power up all sensors on the hip replacement at the same time and then send requests for data from each at different selected times so that with one interrogation signal 128 provided for a set time, such as 1-2 seconds, results in each of the sensors on the hip replacement collecting data during this time period and then, at the end of the period, reporting the data out on respective signals 130 at different times over the next 0.5 to 2 seconds so that with one interrogation signal 128, the data from all sensors 22 is collected.

**[0075]** The interrogation module 124 is operating under control of the control unit 126 which has a microprocessor for the controller, a memory, an I/O circuit to interface with the interrogation module and a power supply. The control unit may output data to a computer or other device for display and use by the physician to treat the subject.

**[0076]** Figure 13 illustrates the operation according to a preferred embodiment within a subject. The subject has an outer skin 132. As illustrated in Figure 13, the interrogation module 124 and control unit 126 are positioned outside the skin 132 of the subject. The interrogation signal 128 passes through the skin of the subject with a wireless RF signal, and the data is received on a wireless RF signal 130 from the sensor (e.g., 22, 22B, 24, 42 and/or 46) back to the interrogation module 124. While the wireless signal can be in any frequency range, an RF range is preferred. A frequency in the VLF to LF ranges of between 3-1300 kHz is preferred to permit the signal to be carried to sufficient depth inside the body with low power, but frequencies below 3 kHz and above 1300 kHz can also be used. The sensing does not require a transfer of large amounts of data and low power is preferred; therefore, a low frequency RF signal is acceptable. This also avoids competition from and inadvertent activation by other wireless signal generators, such as blue tooth, cell phones and the like.

#### **J. COLLECTION, TRANSMISSION, ANALYSIS, AND DISTRIBUTION OF DATA FROM HIP IMPLANTS**

**[0077]** Figure 14 illustrates one embodiment of an information and communication technology (ICT) system 800 arranged to process sensor data (e.g., data from sensor (e.g., 22, 22B, 24, 42 and/or 46) of any one of Figures provided herein). In Figure 14, the ICT system 800 is illustrated to include computing devices that communicate via a network 804, however in other embodiments, the computing devices can communicate directly with each other or through other intervening devices, and in some cases, the computing devices do not communicate at all. The computing devices of Figure 14 include computing servers 802, control units 126, interrogation units 124, and other devices that are not shown for simplicity.

**[0078]** In Figure 14, one or more sensors (e.g., 22, 22B, 24, 42 and/or 46) communicate with an interrogation module 124. The interrogation module 124 of Figure 14 is directed by a

control unit 126, but in other cases, interrogation modules 124 operates autonomously and passes information to and from sensors 22. One or both of the interrogation module 124 and control unit 126 can communicate with the computing server 802.

**[0079]** Within certain embodiments, the interrogation module and/or the control unit may be a wearable device on the subject. The wearable device (e.g., a watch-like device, a wrist-band, glasses or other device that may be carried or worn by the subject) can interrogate the sensors over a set (or random) period of time, collect the data, and forward the data on to one or more networks (804). Furthermore, the wearable device may collect data of its own accord which can also be transmitted to the network. Representative examples of data that may be collected include location (e.g., a GPS), body or skin temperature, and other physiologic data (e.g., pulse). Within yet other embodiments, the wearable device may notify the subject directly of any of a number of prescribed conditions, including but not limited to possible or actual failure of the device.

**[0080]** The information that is communicated between an interrogation module 124 and a sensor (e.g., 22, 22B, 24, 42 and/or 46) may be useful for many purposes as described herein. In some cases, for example, sensor data information is collected and analyzed expressly for the health of an individual subject. In other cases, sensor data is collected and transmitted to another computing device to be aggregated with other data (for example, the sensor data from 22 may be collected and aggregated with other data collected from a wearable device (e.g., a device that may, in certain embodiments, include GPS data and the like).

**[0081]** Figure 14 illustrates aspects of a computing server 802 as a cooperative bank of servers further including computing servers 802a, 802b, and one or more other servers 802n. It is understood that computing server 802 may include any number of computing servers that operate individually or collectively to the benefit of users of the computing servers.

**[0082]** In some embodiments, the computing servers 802 are arranged as cloud computing devices created in one or more geographic locations, such as the United States and Canada. The cloud computing devices may be created as MICROSOFT AZURE cloud computing devices or as some other virtually accessible remote computing service.

**[0083]** An interrogation module 124 and a control unit 126 are optionally illustrated as communicating with a computing server 802. Via the interrogation module 124 or control unit 126, sensor data is transferred to (and in addition or alternatively from) a computing server 802 through network 804.

**[0084]** The network 804 includes some or all of cellular communication networks, conventional cable networks, satellite networks, fiber-optic networks, and the like configured as one or more local area networks, wide area networks, personal area networks, and any other type of computing network. In a preferred embodiment, the network 804 includes any communication hardware and software that cooperatively works to permit users of computing devices to view and interact with other computing devices.

**[0085]** Computing server 802 includes a central processing unit (CPU) digital signal processing unit (DSP) 808, communication modules 810, Input/Output (I/O) modules 812, and storage module 814. The components of computing server 802 are cooperatively coupled by one or more buses 816 that facilitate transmission and control of information in and through computing server 802. Communication modules 810 are configurable to pass information between the computer server 802 and other computing devices (e.g., computing servers 802a, 802b, 802n, control unit 126, interrogation unit 124, and the like). I/O modules 812 are configurable to accept input from devices such as keyboards, computer mice, trackballs, and the like. I/O modules 812 are configurable to provide output to devices such as displays, recorders, LEDs, audio devices, and the like.

**[0086]** Storage module 814 may include one or more types of storage media. For example, storage module 814 of Figure 14 includes random access memory (RAM) 818, read only memory (ROM) 810, disk based memory 822, optical based memory 8124, and other types of memory storage media 8126. In some embodiments one or more memory devices of the storage module 814 has configured thereon one or more database structures. The database structures may be used to store data collected from sensors 22.

**[0087]** In some embodiments, the storage module 814 may further include one or more portions of memory organized a non-transitory computer-readable media (CRM). The CRM is configured to store computing instructions executable by a CPU 808. The computing instructions may be stored as one or more files, and each file may include one or more computer programs. A computer program can be standalone program or part of a larger computer program. Alternatively or in addition, each file may include data or other computational support material for an application that directs the collection, analysis, processing, and/or distribution of data from sensors (e.g., hip replacement sensors). The sensor data application typically executes a set of instructions stored on computer-readable media.

**[0088]** It will be appreciated that the computing servers shown in the figures and described herein are merely illustrative and are not intended to limit the scope of the present invention. Computing server 802 may be connected to other devices that are not illustrated, including through one or more networks such as the Internet or via the Web that are incorporated into network 804. More generally, a computing system or device (e.g., a "client" or "server") or any part thereof may comprise any combination of hardware that can interact and perform the described types of functionality, optionally when programmed or otherwise configured with software, including without limitation desktop or other computers, database servers, network storage devices and other network devices, PDAs, cell phones, wireless phones, pagers, electronic organizers, Internet appliances, television-based systems (e.g., using set-top boxes and/or personal/digital video recorders), and various other products that include appropriate inter-communication capabilities. In addition, the functionality provided by the illustrated system modules may in some embodiments be combined in fewer modules or distributed in additional modules. Similarly, in some embodiments the functionality of some of the illustrated modules

may not be provided and/or other additional functionality may be available.

**[0089]** In addition, while various items are illustrated as being stored in memory or on storage while being used, these items or portions of them can be transferred between memory and other storage devices for purposes of memory management and/or data integrity. In at least some embodiments, the illustrated modules and/or systems are software modules/systems that include software instructions which, when executed by the CPU/DSP 808 or other processor, will program the processor to automatically perform the described operations for a module/system. Alternatively, in other embodiments, some or all of the software modules and/or systems may execute in memory on another device and communicate with the illustrated computing system/device via inter-computer communication.

**[0090]** Furthermore, in some embodiments, some or all of the modules and/or systems may be implemented or provided in other manners, such as at least partially in firmware and/or hardware means, including, but not limited to, one or more application-specific integrated circuits (ASICs), standard integrated circuits, controllers (e.g., by executing appropriate instructions, and including microcontrollers and/or embedded controllers), field-programmable gate arrays (FPGAs), complex programmable logic devices (CPLDs), and the like. Some or all of the systems, modules, or data structures may also be stored (e.g., as software instructions or structured data) on a transitory or non-transitory computer-readable storage medium 814, such as a hard disk 822 or flash drive or other non-volatile storage device 8126, volatile 818 or non-volatile memory 810, a network storage device, or a portable media article (e.g., a DVD disk, a CD disk, an optical disk, a flash memory device, etc.) to be read by an appropriate input or output system or via an appropriate connection. The systems, modules, and data structures may also in some embodiments be transmitted as generated data signals (e.g., as part of a carrier wave or other analog or digital propagated signal) on a variety of computer readable transmission mediums, including wireless-based and wired/cable-based mediums. The data signals can take a variety of forms such as part of a single or multiplexed analog signal, as multiple discrete digital packets or frames, as a discrete or streaming set of digital bits, or in some other form. Such computer program products may also take other forms in other embodiments. Accordingly, the present invention may be practiced with other computer system configurations.

**[0091]** In Figure 14, sensor data from, e.g., sensor (e.g., 22, 22B, 24, 42 and/or 46) is provided to computing server 802.. Generally speaking, the sensor data, represents data retrieved from a known subject and from a known sensor. The sensor data may possess include or be further associated with additional information such as the USI, UDI, a time stamp, a location (e.g., GPS) stamp, a date stamp, and other information. The differences between various sensors is that some may include more or fewer data bits that associate the data with a particular source, collection device, transmission characteristic, or the like.

**[0092]** In some embodiments, the sensor data may comprise sensitive information such as private health information associated with a specific subject. Sensitive information, for example sensor data from sensor (e.g., 22, 22B, 24, 42 and/or 46), may include any information that an

associated party desires to keep from wide or easy dissemination. Sensitive information can stand alone or be combined with other non-sensitive information. For example, a subject's medical information is typically sensitive information. In some cases, the storage and transmission of a subject's medical information is protected by a government directive (e.g., law, regulation, etc.) such as the U.S. Health Insurance Portability and Accountability Act (HIPPA).

**[0093]** As discussed herein, a reference to "sensitive" information includes information that is entirely sensitive and information that is some combination of sensitive and non-sensitive information. The sensitive information may be represented in a data file or in some other format. As used herein, a data file that includes a subject's medical information may be referred to as "sensitive information." Other information, such as employment information, financial information, identity information, and many other types of information may also be considered sensitive information.

**[0094]** A computing system can represent sensitive information with an encoding algorithm (e.g., ASCII), a well-recognized file format (e.g., PDF), or by some other format. In a computing system, sensitive information can be protected from wide or easy dissemination with an encryption algorithm.

**[0095]** Generally speaking, sensitive information can be stored by a computing system as a discrete set of data bits. The set of data bits may be called "plaintext." Furthermore, a computing system can use an encryption process to transform plaintext using an encryption algorithm (i.e., a cipher) into a set of data bits having a highly unreadable state (i.e., cipher text). A computing system having knowledge of the encryption key used to create the cipher text can restore the information to a plaintext readable state. Accordingly, in some cases, sensitive data (e.g., sensor data 806a, 806b) is optionally encrypted before being communicated to a computing device.

**[0096]** In one embodiment, the operation of the information and communication technology (ICT) system 800 of Figure 14 includes one or more sensor data computer programs stored on a computer-readable medium. The computer program may optionally direct and/or receive data from one or more hip replacement sensors implanted in one or more subjects. A sensor data computer program may be executed in a computing server 802. Alternatively, or in addition, a sensor data computer program may be executed in a control unit 126, an interrogation unit 124.

**[0097]** In one embodiment, a computer program to direct the collection and use of hip replacement sensor data is stored on a non-transitory computer-readable medium in storage module 814. The computer program is configured to identify a subject who has a wireless hip replacement inserted in his or her body. The wireless hip replacement may include one or more wireless sensor

**[0098]** In some cases, the computer program identifies one subject, and in other cases, two or

more subjects are identified. The subjects may each have one or more wireless hip replacements, and each wireless hip replacement may have one or more wireless sensors of the type described herein.

**[0099]** The computer program is arranged to direct the collection of sensor data from the wireless hip replacement devices. The sensor data is generally collected with a wireless interrogation unit 124. In some cases, the program communicates with the wireless interrogation unit 124. In other cases, the program communicates with a control unit 126, which in turn directs a wireless interrogation unit 124. In still other cases, some other mechanism is used direct the collection of the sensor data.

**[0100]** Once the sensor data is collected, the data may be further processed. For example, in some cases, the sensor data includes sensitive subject data, which can be removed or disassociated with the data. The sensor data can be individually stored (e.g., by unique sensor identification number, device number, etc.) or aggregated together with other sensor data by sensor type, time stamp, location stamp, date stamp, subject type, other subject characteristics, or by some other means.

**[0101]** The following pseudo-code description is used to generally illustrate one exemplary algorithm executed by a computing server 802 and generally described herein with respect to Figure 14:

Start
Open a secure socket layer (SSL)
Identify a subject
Communicate with a predetermined control unit
Request sensor data from the subject via the control unit
Receive sensor data
If the sensor data is encrypted
THEN decrypt the sensor data
Store encrypted data in the selected storage locations
Aggregate the sensor data with other sensor data
Store encrypted data in the selected storage locations
Maintain a record of the storage transaction
Perform post storage actions
End

**[0102]** Those skilled in the art will recognize that it is common within the art to implement devices and/or processes and/or systems, and thereafter use engineering and/or other practices to integrate such implemented devices and/or processes and/or systems into more comprehensive devices and/or processes and/or systems. That is, at least a portion of the

devices and/or processes and/or systems described herein can be integrated into other devices and/or processes and/or systems via a reasonable amount of experimentation. Those having skill in the art will recognize that examples of such other devices and/or processes and/or systems might include-as appropriate to context and application-all or part of devices and/or processes and/or systems of (a) an air conveyance (e.g., an airplane, rocket, helicopter, etc.), (b) a ground conveyance (e.g., a car, truck, locomotive, tank, armored personnel carrier, etc.), (c) a building (e.g., a home, warehouse, office, etc.), (d) an appliance (e.g., a refrigerator, a washing machine, a dryer, etc.), (e) a communications system (e.g., a networked system, a telephone system, a Voice over IP system, etc.), (f) a business entity (e.g., an Internet Service Provider (ISP) entity such as Comcast Cable, Qwest, Southwestern Bell, etc.), or (g) a wired/wireless services entity (e.g., Sprint, Cingular, Nextel, etc.), etc.

**[0103]** In certain cases, use of a system or method may occur in a territory even if components are located outside the territory. For example, in a distributed computing context, use of a distributed computing system may occur in a territory even though parts of the system may be located outside of the territory (e.g., relay, server, processor, signal-bearing medium, transmitting computer, receiving computer, etc. located outside the territory).

**[0104]** A sale of a system or method may likewise occur in a territory even if components of the system or method are located and/or used outside the territory. Further, implementation of at least part of a system for performing a method in one territory does not preclude use of the system in another territory.

**[0105]** In conclusion, hip replacements utilizing a variety of sensors can be utilized to serve a variety of critical clinical functions, such as safe, accurate and less traumatic placement and deployment of the hip replacement, procedural and post-operative "real time" imaging of hip replacement and the surrounding anatomy, the development of hip replacement complications, and the patient's overall health status. Currently, post-operative (both in hospital and out-patient) evaluation of hip replacement patients is through patient history, physical examination and medical monitoring that is supplemented with diagnostic imaging studies as required. However, most of the patient's recuperative period occurs between hospital and office visits and the majority of data on daily function goes uncaptured; furthermore, monitoring patient progress through the use of some diagnostic imaging technology can be expensive, invasive and carry its own health risks (coronary angiography for example). It can, therefore, be very difficult to accurately measure and follow the development or worsening of symptoms and evaluate "real life" hip replacement performance, particularly as they relate to patient activity levels, exercise tolerance, and the effectiveness of rehabilitation efforts and medications.

**[0106]** At present, neither the physician nor the patient has access to the type of "real time," continuous, objective, hip replacement performance measurements that they might otherwise like to have. Being able to monitor *in situ* hip replacement function, integrity, anatomy and physiology can provide the physician with valuable objective information during office visits; furthermore, the patient can take additional readings at home at various times (e.g. when experiencing pain, during exercise, after taking medications, etc.) to provide important

complementary clinical information to the doctor (which can be sent to the healthcare provider electronically even from remote locations). From the perspective of the patient, being able to monitor many of these same parameters at home allows them to take a more proactive role in their care and recovery and provide him or her with either an early warning indicator to seek medical assistance or with reassurance.

**[0107]** In one alternative, the patient may have a reading device in their home which collates the data from the hip replacement on a periodic basis, such as once per day or once per week. In addition to empowering the patient to follow their own rehabilitation - and enabling them to see the positive (and negative) effects of various lifestyle choices on their health and rehabilitation - such information access can be expected to improve compliance and improve patient outcomes. -For example, within certain embodiments the devices and systems provided herein can instruct or otherwise notify the patient, or a permitted third-party as to deviations (e.g., greater than 10%, 20%, 25%, 50%, 70%, and or 100%) from normal, and/or, set parameters. Furthermore, their recovery experience can be shared via the web with other patients to compare their progress versus expected "norms" for function and rehabilitation and alert them to signs and symptoms that should be brought to their doctor's attention. From a public health perspective, the performance of different hip replacements can be compared in different patients (different sexes, disease severity, activity levels, concurrent diseases such as hypertension and diabetes, smoking status, obesity, etc.) to help manufacturers design better hip replacements and assist physicians in the selection of the right hip replacement for a specific patient types. Payers, patients, manufacturers and physicians could all benefit from the collection of this comparative information. Poor and dangerous products could be identified and removed from the market and objective long-term effectiveness data collected and analyzed. Lastly, data accumulated at home can be collected and transmitted via the Internet to the physician's office for analysis - potentially eliminating unnecessary visits in some cases and encouraging immediate medical follow-up in others.

## REFERENCES CITED IN THE DESCRIPTION

### Cited references

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### Patent documents cited in the description

- [US2004243148A1 \[0010\]](#)
- [WO2008035089A1 \[0010\]](#)
- [US2010100011A1 \[0010\]](#)
- [DE19924676A1 \[0010\]](#)
- [US7383071B \[0032\]](#)
- [US20100285082A \[0032\]](#)
- [US7450332B \[0046\] \[0046\]](#)
- [US7463997B \[0046\]](#)
- [US7924267B \[0046\]](#)
- [US5716981A \[0051\]](#)
- [US20050021126A \[0051\]](#)
- [US20050171594A \[0051\]](#)
- [US20050181005A \[0051\]](#)
- [US20050181009A \[0051\]](#)
- [US20110092948A \[0052\]](#)
- [US20100164705 \[0057\]](#)
- [US7603894B \[0057\]](#)
- [US8283793B \[0059\]](#)
- [US8311632B \[0059\]](#)
- [WO2012061825A \[0069\]](#)

#### Non-patent literature cited in the description

- **ALBERT FOCH**Introduction to BioMEMS CRC Press20130000 [\[0032\]](#)
- **MARC J. MADOU**From MEMS to Bio-MEMS and Bio-NEMS: Manufacturing Techniques and Applications CRC Press20110000 [\[0032\]](#)
- **SIMONA BADILESCU**Bio-MEMS: Science and Engineering Perspectives CRC Press20110000 [\[0032\]](#)
- **STEVEN S. SALITERMAN**Fundamentals of BioMEMS and Medical Microdevices SPIE-The International Society of Optical Engineering20060000 [\[0032\]](#)
- **Bio-MEMS: Technologies and Applications**CRC Press20120000 [\[0032\]](#)
- **VOLKER KEMPE**Inertial MEMS: Principles and Practice Cambridge University Press20110000 [\[0032\]](#)
- **POLLA, D. L. et al.**Microdevices in MedicineAnn. Rev. Biomed. Eng., 2000, vol. 02, 551-576 [\[0032\]](#)
- **YUN, K. S. et al.**A Surface-Tension Driven Micropump for Low-voltage and Low-Power OperationsJ. Microelectromechanical Sys., 2002, vol. 11, 5454-461 [\[0032\]](#)
- **YEH, R. et al.**Single Mask, Large Force, and Large Displacement Electrostatic Linear Inchworm MotorsJ. Microelectromechanical Sys., 2002, vol. 11, 4330-336 [\[0032\]](#)
- **LOH, N. C. et al.**Sub-10 cm<sup>3</sup> Interferometric Accelerometer with Nano-g ResolutionJ.

Microelectromechanical Sys., 2002, vol. 11, 3182-187 [0032]

- **U.K. SINGH et al.** Piezoelectric Power Scavenging of Mechanical Vibration Energy Australian Mining Technology Conference, 2007, 111-118 [0057]
- **CHANDRAKASAN et al.** Next Generation Micro-power Systems 2008 Symposium on VLSI Circuits Digest of Technical Papers, 1-5 [0059]

## PATENTKRAV

1. En kunstig hofteprotese (10) omfattende et femurskaft (20), et femurhoved (18) eller en acetabulumanordning (12, 14), og en eller flere sensorer koblet til nævnte femurskaft, femurhoved eller acetabulumanordning, hvor den kunstige hofteprotese derudover omfatter en hukommelse til lagring af data indsamlet af en eller flere sensorer og placeret i femurskaftet, kendtegnet ved, at nævnte ene eller flere sensorer omfatter et eller flere accelerometre (42, 53).
- 10 2. Kunstig hofteprotese ifølge krav 1, hvor nævnte ene eller flere sensorer derudover omfatter sensorer valgt blandt gruppen bestående af gyroskoper, tryksensorer, kontaktsensorer, positionssensorer, kemiske mikrosensorer, vævsmetaboliske sensorer, mekaniske belastningssensorer og temperatursensorer.
- 15 3. Kunstig hofteprotese ifølge krav 1 eller 2, derudover omfattende: en elektronisk processor placeret inden i femurskaftet, der er elektrisk koblet til den ene eller flere sensorer, eventuelt hvor den elektriske kobling er en trådløs kobling, hvor hukommelsen er koblet til den elektroniske processor og placeret inden i femurskaftet.
- 20 4. Kunstig hofteprotese ifølge ethvert af kravene 1 til 3, hvor den ene eller flere sensorer er placeret inden i protesen.
5. Kunstig hofteprotese ifølge krav 1, hvor nævnte ene eller flere sensorer derudover omfatter kontaktsensorer placeret imellem femurhovedet og acetabulumanordningen, eller acetabulumanordningens udvendige overflade.
- 25 6. Kunstig hofteprotese ifølge krav 1, hvor nævnte ene eller flere sensorer derudover omfatter et flertal af belastningssensorer placeret imellem femurhovedet og acetabulumanordningen, eller hvor acetabulumanordningen omfatter en acetabulumskål eller en acetabulumforing, og nævnte ene eller flere sensorer derudover omfatter belastningssensorer placeret imellem acetabulumforingen og acetabulumskålen.
- 30 7. Kunstig hofteprotese ifølge krav 1, hvor nævnte ene eller flere sensorer derudover omfatter gyroskoper, og accelerometrene eller gyroskoper er placeret på femurskaftet.
- 35 8. Fremgangsmåde til overførsel af data omfattende a) indhentning af data fra den ene

eller flere sensorer i protesen ifølge ethvert af kravene 1 til 7; b) lagring af dataene i hukommelsen ved et lagringssted i protesen; og c) overførsel af data fra hukommelsen til et sted uden for lagringsstedet,

især hvor protesen er implanteret inden i et subjekt, og dataene overføres til et sted

5       uden for subjektet,

især hvor nævnte data overføres til et ur, armbånd, mobiltelefon eller briller; eller et  
hjem eller et kontor; eller en sundhedsplejer.

9.      Fremgangsmåde ifølge krav 8, omfattende:

10     indhentning af kontaktdata fra kontaktsensorerne placeret imellem femurhovedet og  
acetabulumanordningen i protesen ifølge krav 5 placeret in-situ i en patients hofte;  
lagring af kontaktdataene i hukommelsen, hukommelsen er placeret i femurskaftet, der  
er koblet til femurhovedet; og  
overførsel af dataene fra hukommelsen til et sted uden for femurskaftet.

15

10.     Fremgangsmåde ifølge krav 8, omfattende:

indhentning af belastningsdata fra belastningssensorerne placeret imellem  
femurhovedet og acetabulumanordningen i den kunstige hofteprostese ifølge krav 6  
placeret i en patients hofte;

20     lagring af belastningsdataene i hukommelsen, hukommelsen er placeret i femurskaftet,  
der er koblet til femurhovedet; og  
overførsel af belastningsdataene fra hukommelsen i femurskaftet til en hukommelse et  
sted uden for femurskaftet.

25     11.    Fremgangsmåde ifølge krav 8, omfattende:

indhentning af kontaktdata fra en kontaktsensor placeret imellem  
acetabulumanordningen i protesen ifølge ethvert af kravene 2-7 og en bækkenknogle  
hos patienten;  
lagring af kontaktdataene i hukommelsen, hukommelsen er placeret i femurskaftet;  
30     og  
overførsel af kontaktdataene fra hukommelsen i femurskaftet til en hukommelse et sted  
uden for femurskaftet.

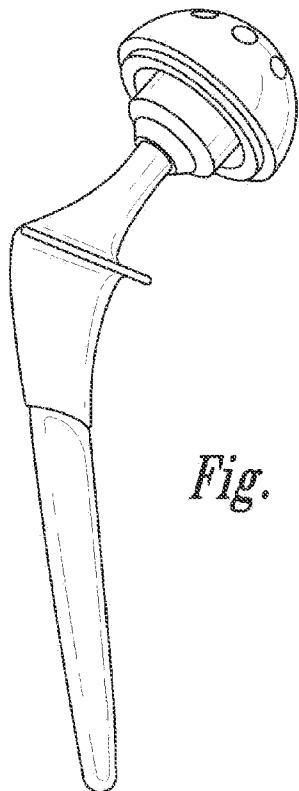
12.     Fremgangsmåde ifølge krav 8, omfattende:

35     indhentning af accelerationsdata fra accelerometeret eller gyroskopet placeret på  
femurskaftet i protesen ifølge krav 7 placeret in-situ i en patients hofte;  
lagring af accelerationsdataene i hukommelsen, hukommelsen er placeret i  
femurskaftet, der er koblet til femurhovedet; og

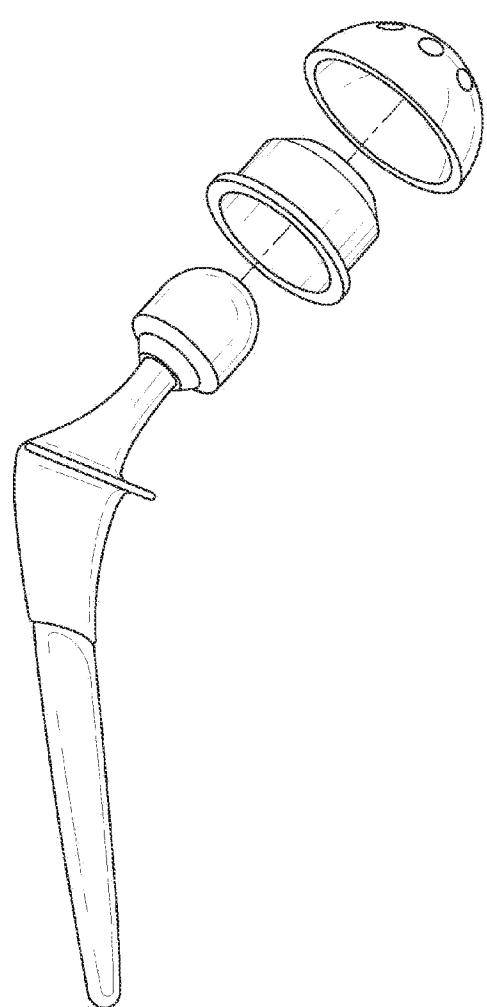
overførsel af accelerationsdataene fra hukommelsen i femurskaftet til en hukommelse et sted uden for femurskaftet.

13. Fremgangsmåde ifølge ethvert af kravene 8 til 12, derudover omfattende trinnet med analysering af dataene.
14. Fremgangsmåde ifølge ethvert af kravene 8 til 13, hvor nævnte data vises grafisk for at muliggøre en visualisering af en ændring over tid, eller vises grafisk for at tilvejebringe et to- eller tredimensionelt billede, eller vises grafisk for at tilvejebringe et bevægeligt to- eller tredimensionelt billede,  
og/eller hvor nævnte data anvendes til at bestemme et bevægelsesområde for et subjekt med en nævnt hofteprotese, eller bestemme eller forudsige vilkårlige mangler eller fejfunktioner i hofteprotesen.
15. Fremgangsmåde til registrering af en forringelse i den kunstige hofteprotese ifølge ethvert af kravene 1 til 7, tilvejebragt for en patient, omfattende trinnet med registrering af en ændring i den ene eller flere sensorer i hofteprotesen, og dermed bestemmelse af forringelsen i hofteprotesen, især hvor nævnte sensor er i stand til at registrere en eller flere fysiologiske parametre og/eller stedparametre.

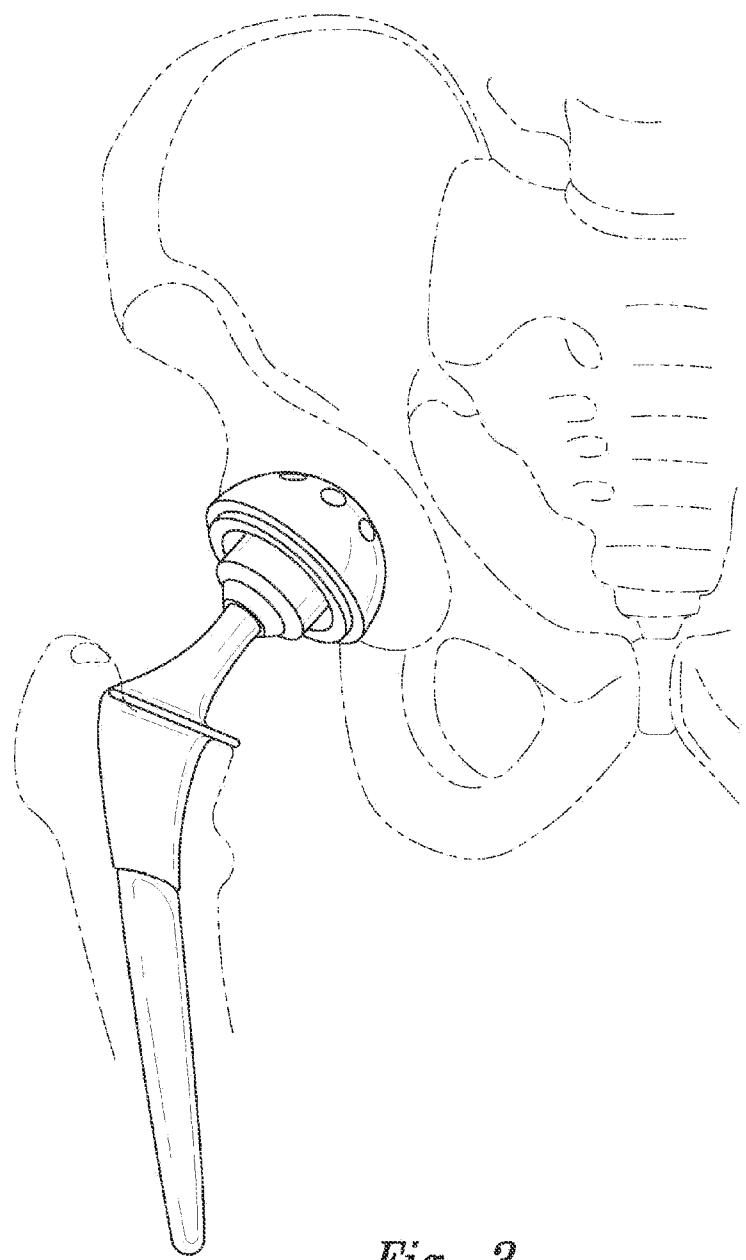
## DRAWINGS



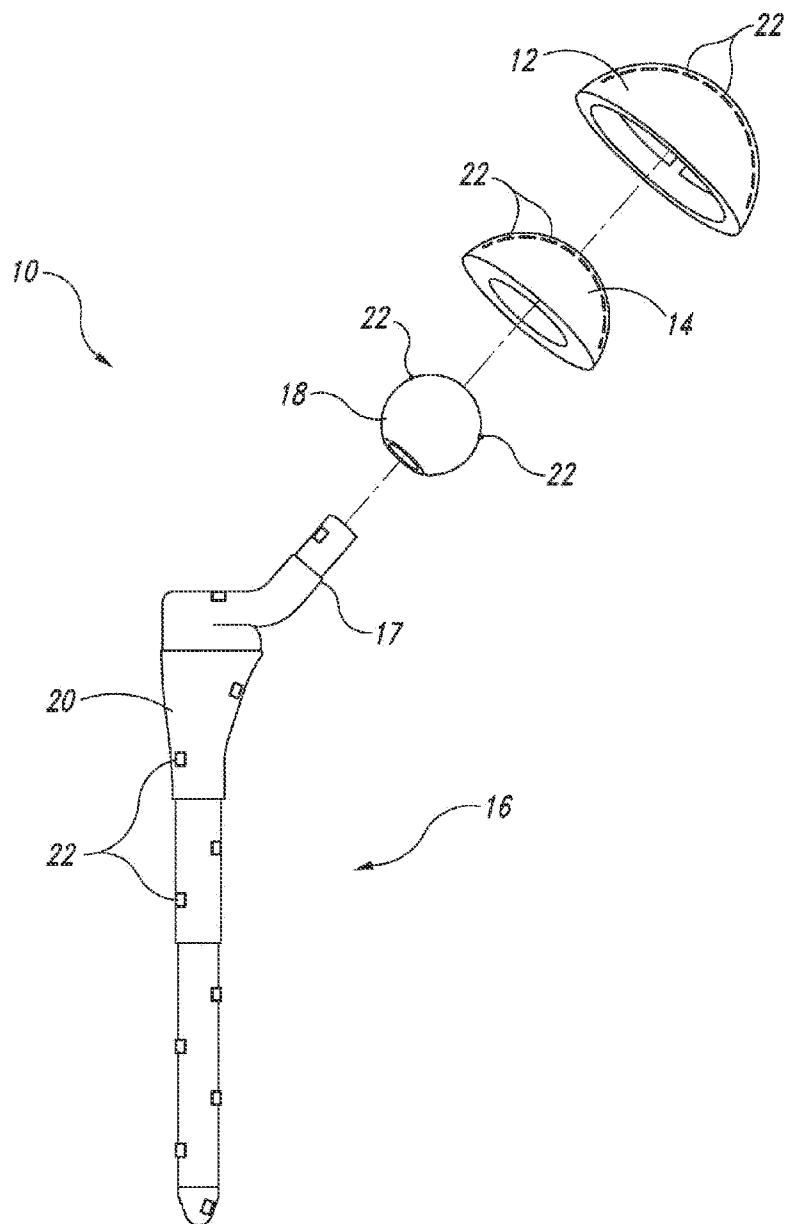
*Fig. 1*



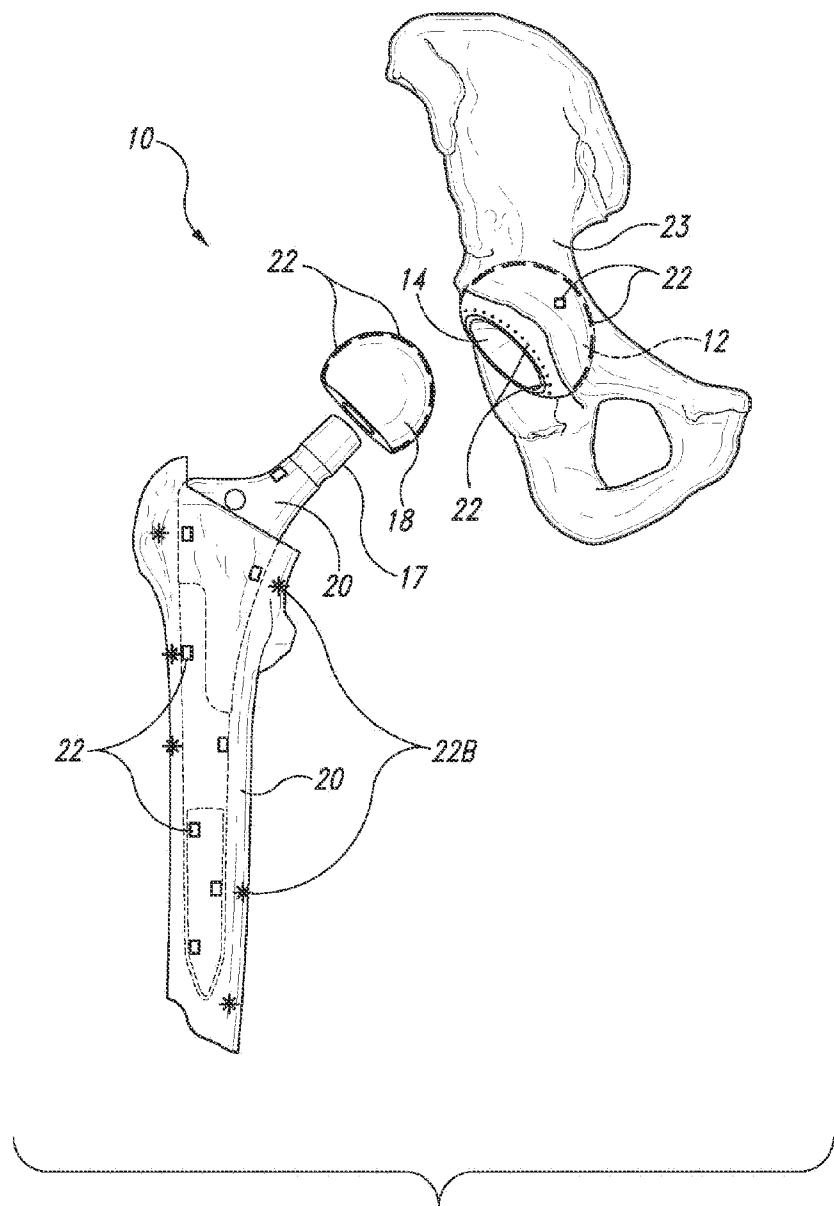
*Fig. 2*



*Fig. 3*



*Fig. 4*



*Fig. 5*

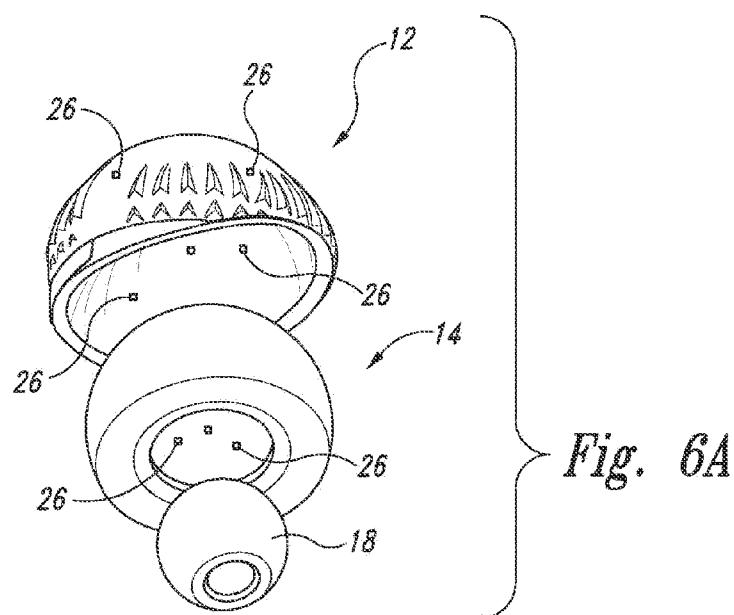


Fig. 6A

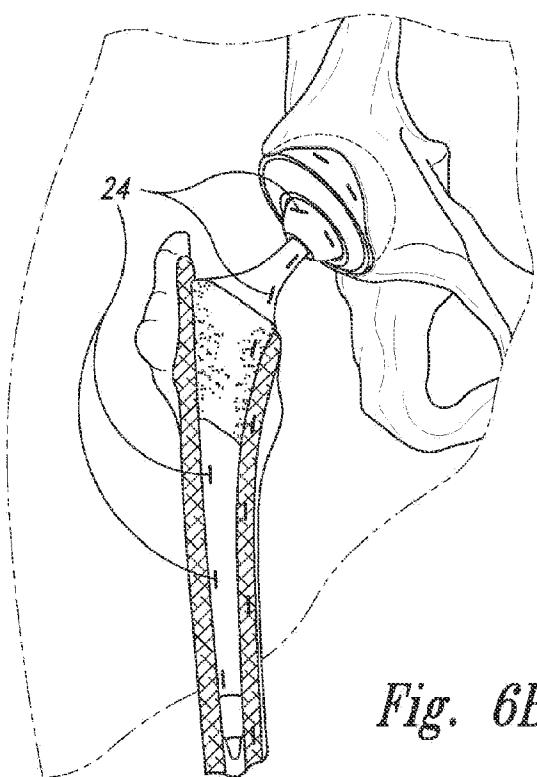
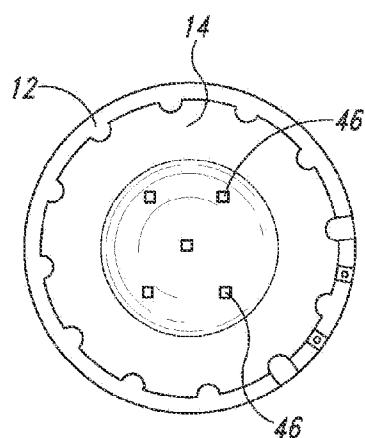
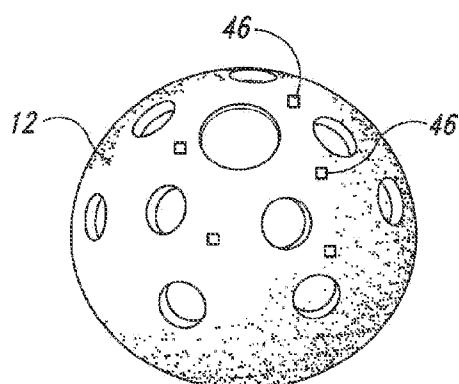
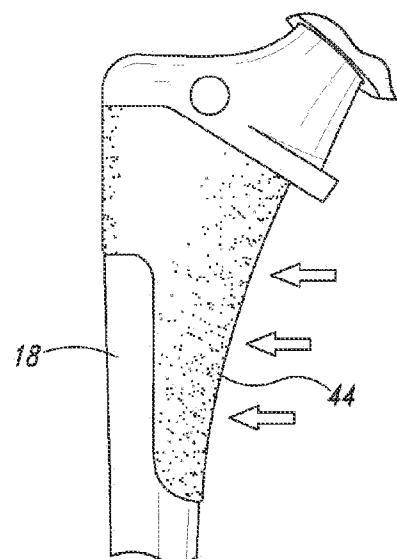
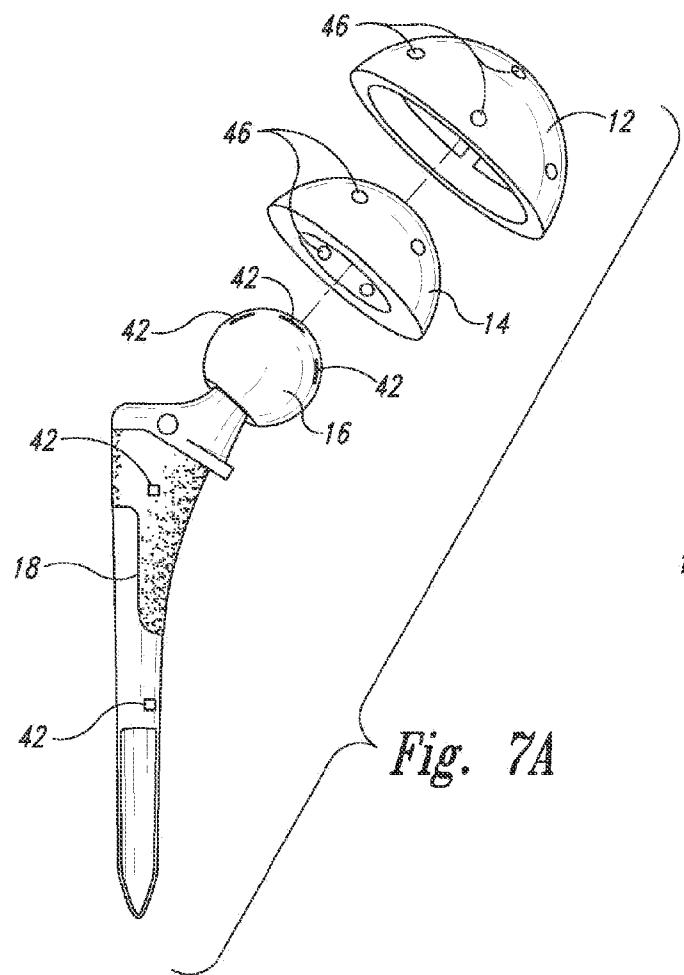
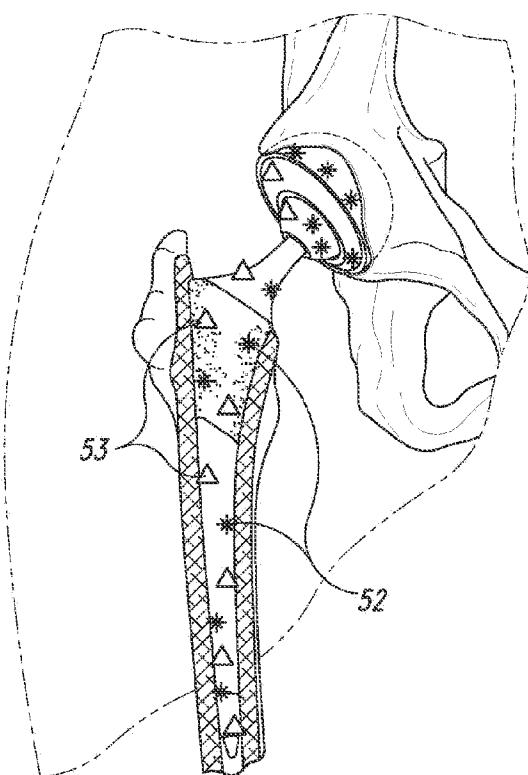
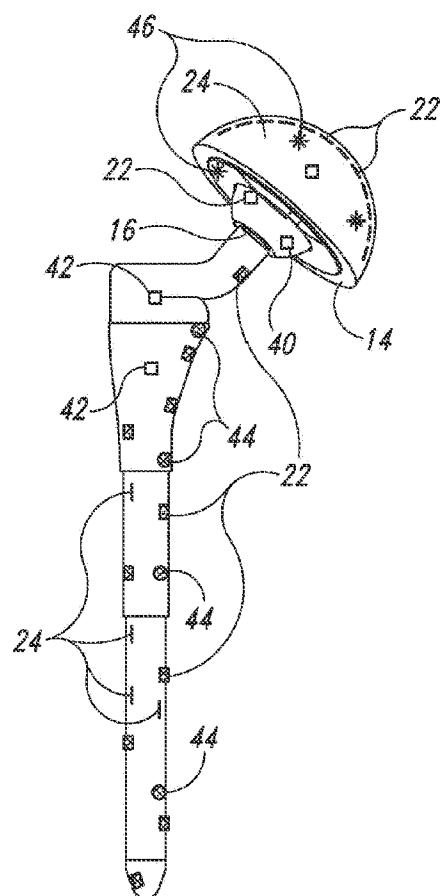
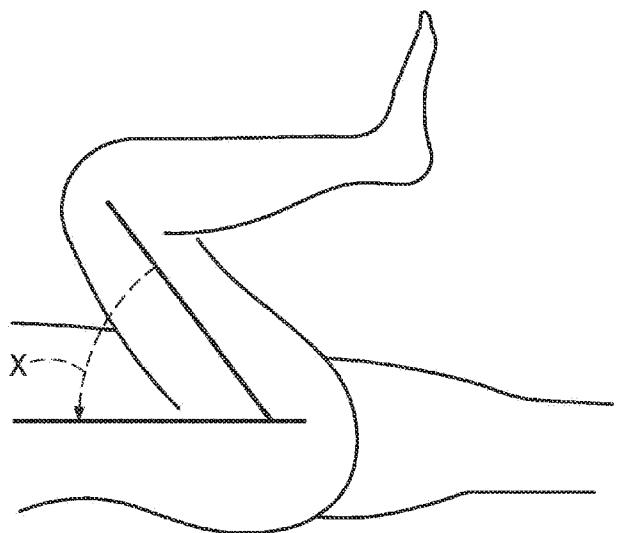


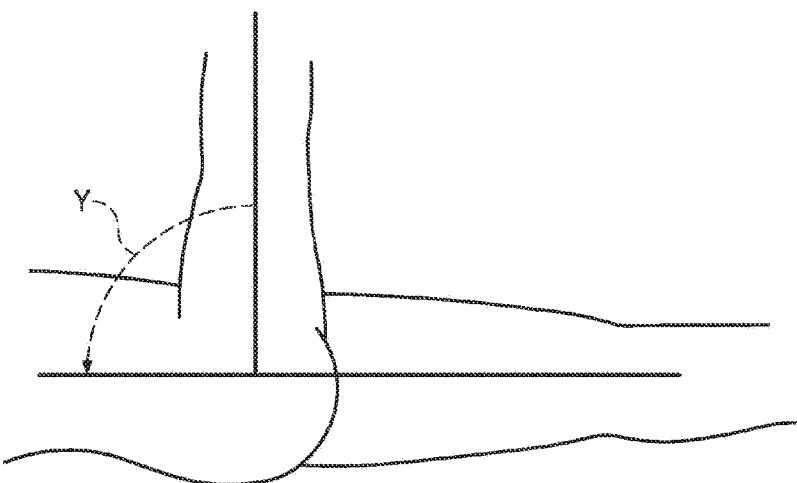
Fig. 6B



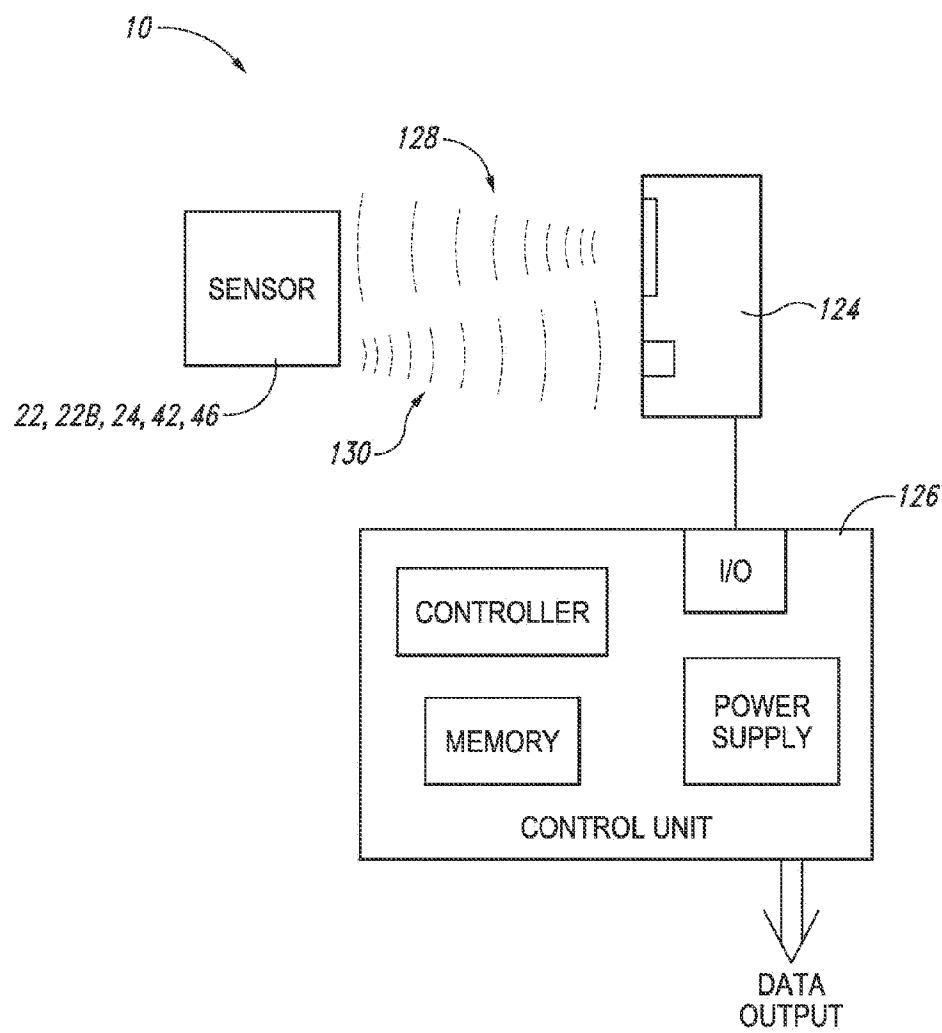




*Fig. 11A*



*Fig. 11B*



*Fig. 12*

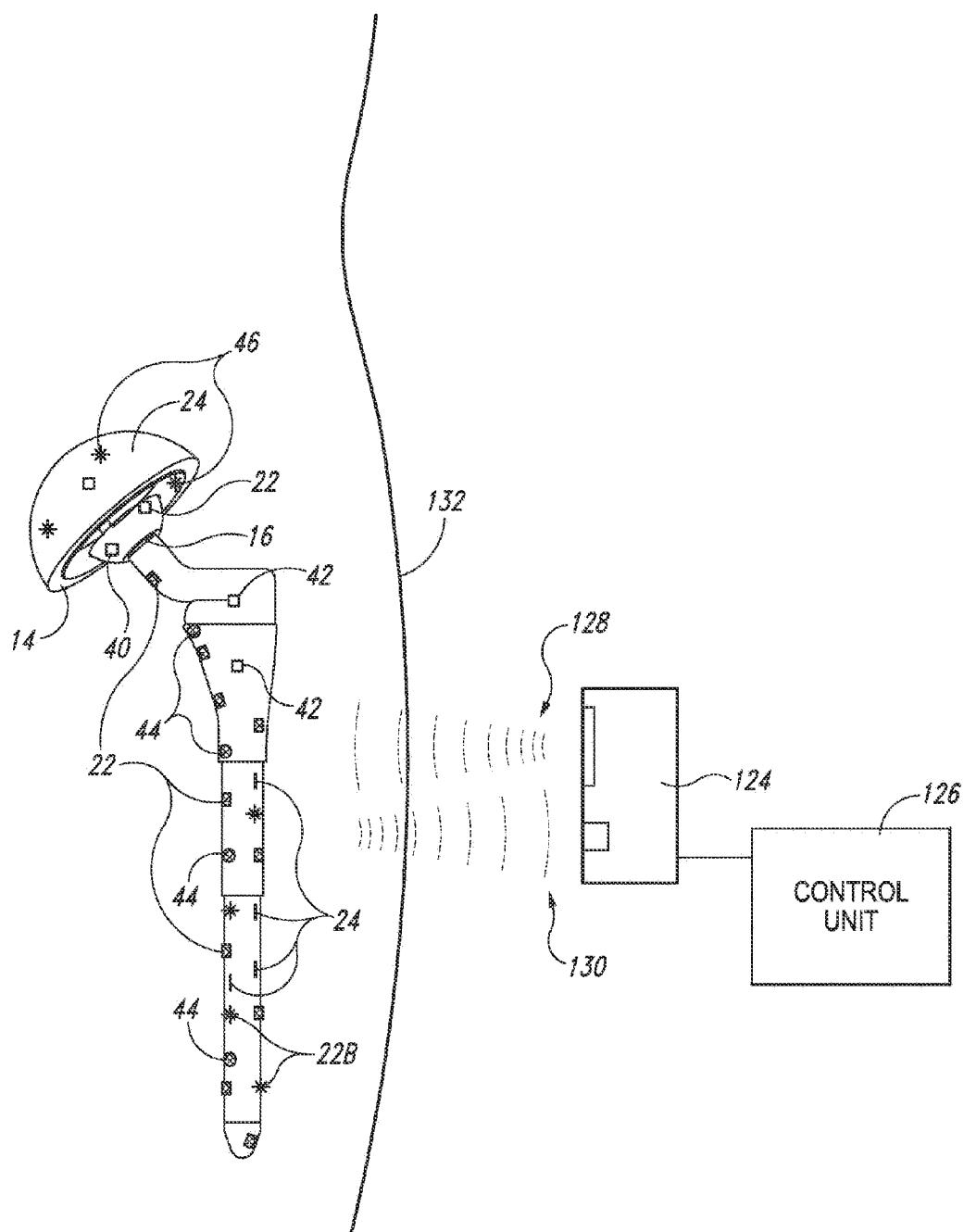


Fig. 13

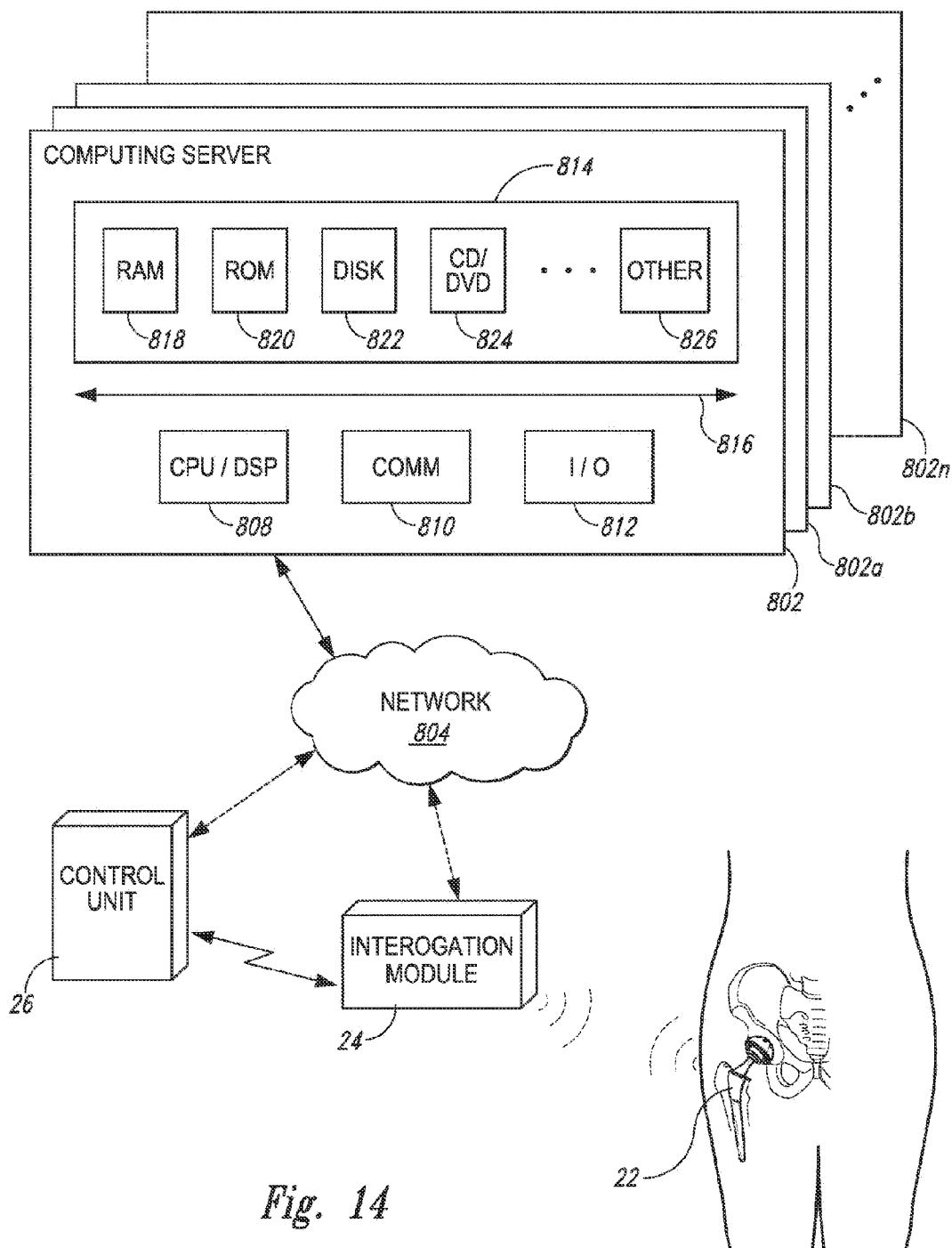


Fig. 14