

(19) **DANMARK**

(10) **DK/EP 3245988 T3**



Patent- og
Varemærkestyrelsen

(12) **Oversættelse af
europæisk patentskrift**

-
- (51) Int.Cl.: **A 61 F 9/00 (2006.01)**
- (45) Oversættelsen bekendtgjort den: **2024-01-29**
- (80) Dato for Den Europæiske Patentmyndigheds bekendtgørelse om meddelelse af patentet: **2023-12-27**
- (86) Europæisk ansøgning nr.: **16170141.2**
- (86) Europæisk indleveringsdag: **2016-05-18**
- (87) Den europæiske ansøgnings publiceringsdag: **2017-11-22**
- (84) Designerede stater: **AL AT BE BG CH CY CZ DE DK EE ES FI FR GB GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL PT RO RS SE SI SK SM TR**
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- (54) Benævnelse: **System til ultralydsforstærket transskleral levering af lægemidler**
- (56) Fremdragne publikationer:
**US-A- 5 016 615
US-A1- 2008 177 220
US-A1- 2010 226 971
US-A1- 2014 276 247
US-A1- 2015 018 752**

DESCRIPTION

[0001] The invention relates to the field of medical devices. In particular to the field of ophthalmic drug delivery devices.

[0002] Throughout this application the terms "drug", "therapeutic agent", and the more general term "molecules" are considered to be interchangeable and the respective use depends on the technical context. The use of one specific wording is not meant to limit the scope of the subject-matter protection is sought for. For example, a therapeutic agent may comprise a drug and/or a drug may comprise molecules.

[0003] The transscleral delivery of drugs is an important aspect of ophthalmic care. For the treatment of many diseases and/or conditions such as central retinal vein occlusion (CRVO), branch retinal vein occlusion (BRVO), central serous retinopathy, cytomegalovirus retinitis (CMV retinitis), retinoblastoma, intraocular lymphoma, ocular melanoma, giant cell arteritis (GCA), histoplasmosis, ischemic optic neuropathy (ION), macular pucker, macular telangiectasia, uveitis, choroidal neovascularization, age-related macular degeneration, diabetic retinopathy, glaucoma, retinitis pigmentosa, macular edema, macular degeneration, multirecurrent pterygia, ocular toxoplasmosis, proliferative vitreoretinopathy (PVR), Stevens-Johnson syndrome (SJS), ocular cicatricial pemphigoid (OIP), ocular degenerative conditions, and a post-surgery conditions, the delivery of a drug into an intrascleral space is necessary.

[0004] However, the eye is a well-protected organ having several natural barriers to prevent foreign substances from entering the posterior segment of the eye. In addition, many of the therapeutic agents for treating posterior segment eye diseases have a high molecular weight and therefore can hardly diffuse across the ocular tissues when applied to the surface of the sclera. In other words an external application is without effect.

[0005] An intravitreal injection is the most commonly used method for drug delivery into an intrascleral space. Although it is accepted by most ophthalmologists as a method of treatment, it is a surgical-level procedure. The intravitreal injection brings risks and problems such as low patient compliance and high time consumption. Furthermore it can only be performed by surgeons and it causes an open wound to the eye that it is prone to infections, and may produce side-effects.

[0006] US 2008 0177220 A1 relates to processes, systems, and apparatuses for transcleral delivery of pharmaceutical formulations to the eye using ultrasound. In one embodiment, a transducer is placed in contact with a coupling media contained in a coupling well in contact with the sclera. When the transducer is placed at a desired standoff distance, ultrasonic waves are emitted to increase tissue porosity and to transport a therapeutic agent through the sclera tissue and into the eye. In another embodiment, a function generator is coupled to an amplifier, a matching network, and a transducer configured to maximize the cavitation effect of ultrasonic waves for drug delivery across a sclera.

[0007] US 20100226971 A1 relates to a system and method for transscleral delivery of therapeutic agents, including macromolecules, into a target site in intrascleral space using ultrasound. The system enhances transscleral diffusivity of macromolecular therapeutic agents and causes little damages to ocular tissues and structure.

[0008] US 5 016 615 A relates to a method and an apparatus for applying a therapeutic substance to body tissue in which ultrasonic radiation is used. The method allows the application of medication, wherein the timing, duration, intensity, and concentration of the application of medication can be adjusted.

[0009] It has been demonstrated that ultrasound based drug delivery methods are a suitable alternative approach for intrascleral drug delivery especially because they do not require an object, e.g., a needle, to be inserted into the eye. However, the corresponding apparatuses are complex and expensive and the corresponding method of use is inconvenient for the patient and the doctor. For example the ultrasound emission from the state of the art is intense and generates cavitation effects and/or heating of the eye tissue. Both of the latter are dangerous and uncomfortable for the patient. Therefore, an improved and non-invasive method for delivering drugs to the posterior segment of the eye is needed.

[0010] Additional advantages, objects, and features of the present invention will be set forth in part in the description which follows and in part will become apparent to those having ordinary skill in the art upon examination of the following or may be learned from practice. The objectives and other advantages may be realized and attained by the structure particularly pointed out in the written description and claims hereof as well as the appended drawings. The above problems are solved by the subject-matter of the independent claim. The dependent claims relate to further aspects of the invention.

[0011] The invention is defined by the features of the independent claim. Preferred embodiments are defined in the dependent claims.

[0012] Described herein is a drug applicator for a system for ultrasound-enhanced transscleral delivery of at least one drug to a target site in an intraocular space, the system comprising a signal generating unit operationally connected to an ultrasound transducer. The drug applicator comprises at least one space holding the drug. The drug applicator is made from a low ultrasound attenuation material. Further, the drug applicator is configured to provide low ultrasound loss coupling of the system to the sclera, and the drug applicator is configured to be mechanically coupled to the system and further configured to be coupled to the ultrasound transducer with low ultrasound loss. The signal generating unit and/or the ultrasound transducer are configured to emit an ultrasound wave form in at least one application cycle, the application cycle comprising at least one ultrasound emitting event with time duration T_A and a waiting period with time duration T_W .

[0013] Further described herein is a system for ultrasound-enhanced transscleral delivery of at

least one drug (molecules) to a target site in an intraocular space. The system comprises a signal generating unit operationally connected to an ultrasound transducer and a drug applicator. The drug applicator comprises at least one space holding the drug. The drug applicator is made from a low ultrasound attenuation material. Further, the drug applicator is configured to provide low ultrasound loss coupling of the system to the sclera, and the drug applicator is configured to be mechanically coupled to the system and further configured to be coupled to the ultrasound transducer with low ultrasound loss. The signal generating unit and/or the ultrasound transducer are configured to emit an ultrasound wave form in at least one application cycle, the application cycle comprising at least one ultrasound emitting event with a time duration TA and a waiting period with time duration TW.

[0014] The term low ultrasound attenuation material relates to any material with an ultrasound attenuation of less than 10 dB/(MHz cm), preferably less than 6 dB/(MHz cm), and more preferably less than 5 dB/(MHz cm). The term low ultrasound coupling loss relates to a coupling between two elements with a loss of less than 20%, preferably less than 10 % at the coupling interface. However, the skilled person realizes that the above numbers reflect what is commonly considered a low value for the respective property.

[0015] In an embodiment of the invention, the drug is provided in a liquid state. In an alternative embodiment, the drug can be encapsulated in hydrophilic substances, e.g., a hydrogel or another similar substance. In an alternative embodiment, the drug can be encapsulated in amphiphilic substances, e.g., amphiphilic nanoparticles or a gel matrix. In an alternative embodiment, the drug can be encapsulated in hydrophobic substances. In an alternative embodiment, the drug can be in a solid form. Depending on the embodiment, it may be advantageous to provide an additional substance to alter at least one physical, chemical, and/or pharmaceutical property of the drug.

[0016] In an embodiment of the invention the drug is selected from the list: antibodies, biologics conjugates, protein drug conjugates, corticosteroid drug conjugates, drug-encapsulated nanoparticles, drug-conjugated nanoparticles, protein drugs, biologics, corticosteroid drugs, nonsteroidal anti-inflammatory drugs, charged molecules, and uncharged molecules.

[0017] In an embodiment of the invention, the ultrasound application cycle is in fact be a single application cycle comprising one ultrasound emitting event with a time duration TA and one waiting period with a time duration TW.

[0018] In an embodiment of the invention, the application cycle is repeated a plurality of times, each of the application cycles comprising one ultrasound emitting event with a time duration TA and one waiting period with a time duration TW. Preferably the application cycle is repeated 2 to 10 times, more preferably 4 times.

[0019] In an embodiment of the invention the different application cycles have different ultrasound emitting durations and different wait time durations.

[0020] The drug applicator may be configured to be exchangeable and/or may be designed for a single use application.

[0021] In an embodiment of the invention, at least one surface of the drug applicator and at least one surface of the ultrasound transducer and/or an application head which comprises the ultrasound transducer are formed to receive each other and to facilitate a coupling. Preferably the coupling is a positive-fitting and/or a friction-locked connection; however, there are also other coupling methods to be used. An exchangeable drug applicator is designed to be coupled and decoupled multiple times to the system and a single use drug applicator is designed to be coupled and decoupled at least one time to the system.

[0022] In an embodiment of the invention, at least one surface of the ultrasound transducer and/or the application head comprising the ultrasound transducer is formed to receive differently formed drug applicators.

[0023] In an embodiment of the invention, the outer appearance of the drug applicator is indicating the contained drug. In this embodiment the outer appearance relates a shape of at least one surface, preferably the coupling surface, and/or at least one human- or machine-readable label. Additionally or alternatively color coding is used to indicate the contained drug.

[0024] In an embodiment of the invention, the drug receiving space is substantially sealed at a surface designated for coupling with the sclera and the seal is configured to allow for drug permeation.

[0025] In one embodiment of the invention, the drug applicator comprises a drug receiving space that is closed to an exterior space, thereby sealing off the drug from any undesired contact with outside gases or substances. In this embodiment the at least one of the sealing surfaces preferably is configured to allow for drug permeation preferably during the ultrasound application or wait period of the application cycle.

[0026] In another embodiment of the invention, the drug receiving space is substantially open at a surface designated for coupling with the sclera.

[0027] In one embodiments of the invention the drug receiving space is substantially sealed prior to use, i.e., during fabrication, storage, and/or transport. At least one surface is preferably configured such that the seal is completely or partially removed prior to use thereby forming an opening at a surface designated for coupling with the sclera.

[0028] In an embodiment of the invention, the drug applicator is configured to be filled and/or refilled, and wherein the drug applicator receives between 10 μ L and 1 mL of the drug and optionally at least one additional substance.

[0029] In one embodiment of the invention, the drug receiving space is an empty space. The

empty space is configured to be filled with the drug. The filling is, e.g., performed with an injection needle and the drug applicator is essentially self sealing the needle hole after the drug has been injected into the drug receiving space and the needle has been removed. Alternatively, the filling can be performed using a port structure formed at the drug applicator. The port structure is configured to receive a needle and/or drug container and has a channel allowing for filling the drug into the drug receiving space. Furthermore, the port structure is preferably configured to seal the drug receiving space after the drug has been inserted.

[0030] In one embodiment of the invention the drug receiving space is substantially open at a surface designated for coupling with the sclera. In this and any similar embodiment the drug receiving space is preferably filled directly using the opening at a surface designated for coupling with the sclera.

[0031] In one embodiment of the invention at least one additional substance is filled into the drug receiving space, e.g. an ultrasound coupling agent.

[0032] In the system according to any of the embodiments, the drug applicator may be made from an elastic material having Young's modulus of less than 10 GPa.

[0033] According to the present invention the design of the drug applicator is not dictated by the ultrasound transmission properties. In particular, no defined stand-off distance between the ultrasound transducer and the sclera has to be maintained. Instead the design is variable and is preferably optimized to enable a low loss coupling and a pleasant user experience.

[0034] In one embodiment of the invention, the drug applicator is relatively soft and adapts to different application angles and different shapes of the eye. Therefore the usability is optimized.

[0035] The drug applicator may be made from at least one of the following materials: epoxy resin, polyurethane rubber, polycarbonate, nylon 6 - 6, polyvinyl chloride, polyester, ultra-high molecular weight polyethylene, polypropylene, Teflon, polystyrene, neoprene rubber, polyvinyl alcohol, polydimethylsiloxane, silicone-containing rubber, silicon hydrogel, silicone rubber. Still in the same aspect of the invention the drug applicator is additionally or alternatively made from silicon rubber doped with at least one of the following materials: nickel, silver, palladium, tungsten, gold, platinum, silicon oxide, titanium oxide, aluminum oxide, barium sulphate, iron oxide, zirconium dioxide, cerium oxide, bismuth oxide, ytterbium oxide, lutetium oxide, hafnium oxide.

[0036] The system may further comprise a controller, wherein the controller is configured to control at least one of a plurality of parameters of the application cycle, the plurality parameters of the application cycle are selected from the following: the time duration TA of the ultrasound emitting event, the time duration TW of the wait period after the ultrasound emitting event, the number of application cycles, the intensity of the ultrasound emitting event, the central frequency of the ultrasound emitting event, the mechanical index of the ultrasound emitting

system, and in case of a pulsed ultrasound emitting event: the repetition rate of the ultrasound emitting event and the duty cycle of the ultrasound emitting event.

[0037] In an embodiment of the invention, the controller is operationally connected with at least one of the following: the application head, the signal generating unit, the ultrasound transducer, and the drug applicator. The connection is preferably wireless or with a cable.

[0038] In an embodiment of the invention, the ultrasound signal has in sine wave form at a central frequency between 20 kHz and 100 kHz, preferably at 40 kHz. In one embodiment of the invention, the ultrasound signal has a spatial average temporal average intensity no greater than 4 W/cm², preferably in the range between 0.005 W/cm² and 1 W/cm². In one embodiment of the invention, the ultrasound emitting device and/or the controller is configured such that continuous or pulsating waves are generated and the ultrasound is applied as pulsating waves with a duty cycle preferably ranging from 30% to 0% with a pulse repetition rate preferably between 1Hz to 100Hz.

[0039] In an embodiment of the invention, the mechanical index of the ultrasound application cycle does not exceed 0.20 to avoid violent effects and tissue damage induced by the ultrasound. The mechanical index predicts the cavitation activities during the ultrasound application period at a particular combination of frequency and intensity. The mechanical index is therefore preferably controlled by the frequency and intensity of the ultrasound emission.

[0040] In an embodiment of the invention, the system may further comprise an information receiving and/or sending unit. The information receiving and/or sending unit may be configured to receive and/or send information related to the drug. The information receiving and/or sending unit can be operationally connected to the signal generating unit and/or the controller. Alternatively, the information receiving and/or sending unit can be operationally connected to the signal generating unit and/or the controller and the controller configured to control at least one of a plurality of parameters of the application cycle based on the information related to the drug. The information related to the drug is preferably stored on the drug applicator.

[0041] In order to be delivered effectively, different types of drug may require different parameters of the application cycle. In an embodiment of the invention, the system is able to receive information from the drug applicator and identify the drug applicator and thus identify the type of drug and control the different parameters of the application cycle accordingly.

[0042] The information related to the drug and/or the drug applicator can be stored in, at, and/or on the drug applicator using different methods and requiring different methods for the information sending and/or receiving unit to retrieve the information from the drug applicator.

[0043] In an embodiment of the invention a lock and key method is used to identify the drug applicator. At least one surface of the drug applicator and at least one corresponding surface of the application head having a matching shape to allow for a positive locking connection. Due to the positive locking the drug applicator is identified and the different parameters of the

application cycle are controlled accordingly. Positive-locking of more than one different drug applicator is possible, preferably using different locking-surfaces on the application head. The different drug applicators lock in a different end position and the information about the drug applicator is coded in the different end positions and is retrieved by the information receiving and/or sending unit.

[0044] In an embodiment of the invention a human- and/or machine-readable label is used to store the information about the drug applicator. Accordingly, the information receiving and/or sending unit would comprise respective means for reading the human- and/or machine-readable label. Alternatively or additionally, an RFID chip in or on the drug applicator is preferably used to store the information about the drug applicator. Accordingly the information receiving and/or sending unit would comprise an RFID reader.

[0045] The information about the drug applicator preferably contains at least one of the following information: information about the drug in the drug applicator, information about the shelf life of the drug, information about the application cycle.

[0046] The above lists are not intended to limit the scope of the subject-matter protection is sought for. The skilled person will conceive a plurality of improvements and/or variations of the above solutions once presented with the problem of storing information on the drug applicator.

[0047] In an embodiment the drug applicator is filled with a drug from a container holding several doses of the drug. In this embodiment the information sending and/or receiving unit is configured to receive the information about the drug from the container.

[0048] In an embodiment of the invention, when the drug comprises molecules with a size of 70 kDa or less, the controller is configured to control the time duration TA to be between 30 s and 300 s and the drug applicator is configured such that the drug transit through the sclera during the time duration TA. Additionally or alternatively, when the drug comprises molecules with a size of more than 70 kDa, the controller is configured to control the time duration TW to be between 60 s and 600 s and the drug applicator is configured such that the molecules drug transit through the sclera during the time duration TW.

[0049] It is an embodiment of the invention that the effectiveness of the delivery is dependent on the molecule size. For relatively small molecules, preferably smaller than 70 kDa, the penetration rate and/or depth is effectively controlled by controlling the duration of the ultrasound emission event of the at least one application cycle. For relatively large molecules, preferably larger than 70 kDa, the penetration rate and/or depth is controlled effectively by controlling the duration of the wait period after the ultrasound emission event of the at least one application cycle. Therefore for each drug an optimal set of parameters for the application cycle can be found.

[0050] In an embodiment of the invention, optimal sets of parameters of the application cycle for different drugs are stored in the system. Additionally or alternatively, the optimal sets may

be added, modified, or deleted by a user and/or a remote access using connecting means. The system is preferably further connected to a central database, the database being configured to manage and distribute the optimal sets.

[0051] In an embodiment of the invention, the optimal set of parameters of the application cycle for the respective drug that is contained within the drug applicator is stored at, in and/or on the drug applicator itself and can be retrieved with the information receiving/sending unit.

[0052] In an embodiment of the invention, the system further comprises display and/or manual input unit configured to display and/or manually set at least one of the plurality parameters of the application cycle.

[0053] In certain situations, e.g., specific individual conditions of the eye to be treated, it is necessary to change at least one of the plurality parameters of the application cycle manually. In one embodiment of the invention the system comprises a display unit that is configured to display the parameters of the application cycle and preferably other information assisting the user. In one embodiment of the invention the system comprises, additionally or alternatively to the display unit a manual input unit to set at least one of the plurality parameters of the application cycle.

[0054] The display unit and the manual input unit are preferably combined in one unit, e.g., in a touch-screen device. The display unit and/or the manual input unit are integrated with the system or coupled to the system with connecting means. Connecting means preferably comprise a cable and/or wireless connection.

[0055] In an embodiment of the invention, the system further comprises a temperature sensor configured to sense the temperature of the surface of the sclera, preferably a thermocouple and/or an infrared thermometer. And the controller is configured to control the ultrasound emission event such that during the time T_A the temperature of the surface of the sclera does not increase by more than 1°C .

[0056] The heating of the sclera surface is a critical aspect of ultrasound enhanced delivery of drugs to a target site in the intraocular space. In one embodiment of the invention is the heating of this sclera is measured. The heating can be measured using different methods known to the skilled person.

[0057] In an embodiment of the invention and infrared thermometer is used for measuring the heating of an area of the sclera where the ultrasound applied, during a time when the ultrasound is applied. In one embodiment of the invention a thermocouple is used to measure the heating of an area of the sclera where the ultrasound is applied, during a time when the ultrasound is applied.

[0058] In an embodiment of the invention the parameters of the application cycle are controlled such that the heating of an area of the sclera where the ultrasound is applied, during

a time when the ultrasound is applied, does not exceed 1°C, advantageously it does not exceed 0.5°C. Preferably, the intensity and/or the application time TA are controlled to control the heating of the sclera.

[0059] Further described herein is a method for using the system of any one of the above aspects and embodiments of the invention to deliver drugs to a target site in the intraocular space. The method for the delivery of a drug to a target site in an intraocular space may comprise the steps of providing a drug applicator and/or a system according to any one of the above aspects and/or embodiments, coupling the drug applicator to a surface of the sclera, and applying at least one ultrasound application cycle, wherein the application cycle comprises an ultrasound application with a time duration TA and a waiting period with a time duration TW.

[0060] The step of coupling the system to the eye may comprise applying a pressure to the drug applicator and pressing the drug applicator to the surface of the sclera.

[0061] The drug applicator is formed from a soft and elastic material. To couple the drug applicator to the eye, the user and/or doctor may press the drug applicator to the eye. The drug applicator is elastically deformed upon contact with the surface of the sclera and thereby forming an interface between the drug applicator and the surface of the sclera. The interface is preferably increased in size when the pressure is increased. The material of the drug applicator has to be adapted to not cause an unpleasant sensation to the eye. Adaptation preferably comprises any selection of the following: adapting the elasticity, adapting the temperature and/or adapting the structure.

[0062] The step of coupling the system to the eye may additionally comprise the step of applying an ultrasound coupling agent to the drug applicator and/or to the surface of the sclera prior to pressing the drug applicator to the surface of the sclera. Applying an ultrasound coupling agent to the drug applicator and/or to the surface of the sclera prior to pressing the drug applicator to the surface of the sclera may improve the transmission of the ultrasound signal to the sclera tissue.

[0063] The step of providing a drug applicator and/or a system may additionally comprise the step of loading a drug into the drug applicator.

[0064] The drug applicator may form a cartridge that is designed to be attached to the system.

[0065] The drug applicator does not necessarily permanently hold a drug. The drug is loaded into the drug applicator prior to the ultrasound application. The loading can be performed using any of the above described methods of filling the drug applicator with an injection needle, a port structure, and/or a direct filling method.

[0066] The step of providing a drug applicator and/or a system additionally or alternatively may comprise the step replacing an empty drug applicator with a pre-loaded drug applicator.

[0067] The drug applicator may be pre-loaded with the drug. An empty or blank drug applicator and/or empty previous used drug applicator is removed from the system and a pre-loaded drug applicator is coupled to the system prior to the ultrasound application.

[0068] The method may additionally comprise the step of determining the plurality of parameters of the application cycle, comprising at least the number of application cycles the time durations TA and TW, by the information about the drug received from the information sending and/or receiving unit.

[0069] The plurality of parameters of the application cycle, comprising at least the number of application cycles the time durations TA and TW, may be manually inputted by a user.

[0070] The temperature of the surface of the sclera may be measured during the application time TA, and the controller controls the ultrasound emission such that the temperature increase of the surface of the sclera does not exceed 1°C, advantageously it does not exceed 0.5°C.

[0071] Further features, expediciencies and advantageous refinements become apparent from the following description of the exemplary embodiment in connection with the figures. In the Figures:

Fig. 1 shows an embodiment of the system for ultrasound enhanced transscleral delivery of drugs;

Fig. 2 shows details of an embodiment of the delivery unit;

Figs. 3a to 3d show different embodiments of the drug applicator;

Fig. 4 shows a perspective view of an embodiment of an application head of the system;

Fig. 5 shows a perspective view of a system according to the present description;

Fig. 6 shows a perspective view of a system according to the present description; and

Fig. 7 shows a perspective view of a system according to the present description.

[0072] Like elements, elements of the same kind and identically acting elements may be provided with the same reference numerals in the figures. In the description of the embodiments only features of the respective embodiment which have not been described before are explicitly mentioned. The skilled person is able to realize which features of other embodiments are required to exercise the invention.

[0073] Fig. 1 shows one embodiment of the system for ultrasound enhanced transscleral delivery of drugs. The system comprises a delivery unit 200, a signal generating unit 300, and an input and control unit 400. The delivery unit 200, the generating unit 300, and the input and

control unit 400 are operationally interconnected by connecting means 501, 503, 504. Connecting means may comprise wired and wireless connection means. Preferred connection means are a WiFi, or Bluetooth, and/or any kind of bus connection.

[0074] The delivery unit 200, the generating unit 300, and the input and control unit 400 are preferably integrated together into a single housing and/or are optionally arranged into functional groups and integrated into a number of housings. For example, the input and control unit 400 is preferably formed as a hand-held device comprising display and input means; the delivery unit 200 is preferably formed as a compact, optionally a hand-held, device that is configured to be ergonomically placed in front of the eye 100 and is further configured to touch the scleral surface; and the signal generating unit 300 is preferably formed in a rugged housing, preferably having a rack compatible form factor.

[0075] Details of one embodiment of the delivery unit 200 are shown in Figure 2 . The delivery unit 200 comprises a drug applicator 201, an ultrasound transducer 202, and preferably an information sending and receiving unit 203. The drug applicator 201 comprises at least one space 800 to hold the drug. The term ultrasound transducer 202 is including any hardware to produce an ultrasound signal.

[0076] The drug applicator 201 is formed from a low ultrasound attenuation material. The low ultrasound attenuation material can be at least one selected from the following list: epoxy resin, polyurethane rubber, polycarbonate, nylon 6-6, polyvinyl chloride, polyester, ultra-high molecular weight polyethylene, polypropylene, Teflon, polystyrene, neoprene rubber, polyvinyl alcohol, polydimethylsiloxane, silicone-containing rubber, silicon hydrogel, silicone rubber. Additionally or alternatively the drug applicator 201 can be formed from a silicon rubber doped with at least one of the following materials: nickel, silver, palladium, tungsten, gold, platinum, silicon oxide, titanium oxide, aluminum oxide, barium sulphate, iron oxide, zirconium dioxide, cerium oxide, bismuth oxide, ytterbium oxide, lutetium oxide, hafnium oxide.

[0077] In an embodiment of the invention, the drug applicator 201 is configured to be coupled to the scleral surface with a low ultrasound loss at a surface 601b directed towards the eye 100. To enhance ultrasound coupling a substance may be applied to the surface 601b and/or the scleral surface of the eye 100. The substance is filling an optional gap 601a between the drug applicator 201 and the scleral surface of the eye 100. The substance can be, for example, an ultrasound coupling agent.

[0078] In an embodiment of the invention, coupling of the drug applicator 201 to the scleral surface can be improved by the design of the drug applicator 201. The drug applicator 201 is formed from an elastic material having a Young's modulus of less than 10 GPa. When the drug applicator 201 is made from a sufficiently elastic material, the drug applicator can be pressed against the eye 100 and, upon exerting a pressure, the drug applicator 201 will deform and adapt to the specific form of an individual eye 100. The pressure can be evenly distributed on the scleral surface and the user experience is improved. In addition, the gap 601 a between the scleral surface and the drug applicator 201 is minimized and the ultrasound coupling is

improved.

[0079] It is an advantage of the present invention over the prior art, that the delivery performance is not influenced by the stand-off distance d of the drug applicator 201. Therefore, deformation of the drug applicator 201 is possible, without compromising the drug delivery performance.

[0080] The drug applicator 201 is configured to be mechanically coupled to the drug delivery system. The drug applicator 201 is configured to be coupled to the ultrasound transducer 202. The coupling comprises a mechanical coupling and may hold the drug applicator 201 in a fixed position relative to the ultrasound transducer 202, preferably in a fixed position at the ultrasound transducer 202. The coupling may further comprise a low loss ultrasound coupling of the drug applicator 201 to the ultrasound transducer 202. The low loss ultrasound coupling is preferably improved by using a substance at an interface 602 between the drug applicator 201 and the ultrasound transducer 202. The substance is preferably an ultrasound coupling agent. The mechanical coupling preferably is a releasable mechanical coupling that is designed for coupling different drug applicators 201 to the ultrasound transducer 202. The different drug applicators 201 preferably have a different size and/or a different form factor.

[0081] In an embodiment of the invention, the information sending and/or receiving unit 203 is arranged and configured such that the information sending and/or receiving unit 203 can retrieve information about the drug applicator 201 and/or the drug when the drug applicator is coupled to the application head. In order to be able to identify the drug applicator 201, the information sending and/or receiving unit 203 comprises reading means configured to read information related to the drug applicator 201. The reading means preferably include a reader for a human- or machine-readable label and/or an RFID label.

[0082] Figures 3a to 3d show different embodiments of the drug applicator 201. It is preferred that the drug held in the drug receiving space 800 is sealed towards an exterior space, i.e. the ambient, to protect the drug from being polluted by any foreign substance or gas. The protection may be particularly desirable during production, transport, and storage of the drug applicator 201 or the system. Directly before use the seal may be broken to allow for the drug in the space 800 to be delivered.

[0083] In the embodiment of Figure 3a, the drug applicator 201 is sealed on all surfaces. It is preferred that the space 800 for holding the drug inside the drug applicator 201 of this embodiment is filled with a drug during the production process of the drug applicator 201.

[0084] In the embodiment of Figure 3b, the drug applicator 201 is sealed on all surfaces and comprises a port structure 201c. The port structure 201c is configured to allow filling and/or refilling of this space 800 with a drug.

[0085] In the embodiment of Figure 3c, the drug applicator 201 has at least one opening at a surface directed towards the scleral surface. It is preferred that the drug receiving space 800 is

configured to be filled through at least one opening at the surface directed towards the scleral surface.

[0086] In the embodiment of Figure 3d, the drug applicator has at least one opening at a surface directed towards the scleral surface and a port structure 201c. The port structure 201c is configured to allow filling and/or refilling of this space 800 with a drug.

[0087] In these embodiments, one surface, preferably a surface directed towards the scleral surface of the eye 100, is preferably configured to have a peel-of-cover and/or is configured to be permeable for the drug held in this space 800.

[0088] In an embodiment of the invention, the drug receiving space 800 is configured to receive a volume of a drug. The volume of the drug is preferably ranging from 10 μ L to 1 mL. Additionally or optionally a further substance can be inserted into the drug receiving space 800 to improve the delivery of the drug and/or improve at least one chemical, physical and/or pharmaceutical property of the drug.

[0089] In an embodiment of the port structure 201c, the port structure is configured to be pierced by an injection needle. The injection needle allows liquid communication between the drug receiving space 800 and a drug reservoir or container coupled to the injection needle. The drug is preferably inserted from the drug reservoir or container into the drug receiving space 800 by applying a pressure. It is preferred that the port structure 201c is self-sealing after the injection needle has been removed.

[0090] The signal generating unit 300, as shown in Figure 1, comprises a controller 302 and a signal generator and/or amplifier 301. The controller 302 is operationally connected to the signal amplifier 301. The signal generator and/or amplifier 301 are operationally connected with the ultrasound transducer 202 by connecting means 501. The signal generator and/or amplifier 301 and the controller 302 are preferably arranged in a common housing 303 of the signal generating unit 300.

[0091] In an embodiment of the invention, the controller 302 is configured to control the signal generator and/or amplifier 301 to generate the ultrasound signal. Additionally or optionally the signal generator and/or amplifier 301 is configured to amplify the ultrasound signal. The emitted ultrasound signal has preferably sine wave form and has a central frequency between 20 kHz and 100 kHz, more preferably at 40 kHz.

[0092] In an embodiment of the invention, the emitted ultrasound signal consists of pulsating waves with a duty cycle preferably ranging from 30% to 70% at a preferred pulse repetition rate between 1 Hz and 100 Hz.

[0093] In an embodiment of the invention, the mechanical index of the emitted ultrasound signal is preferably not exceeding 0.2 to avoid violent effects, e.g., cavitation effects, and/or tissue damages induced by the emitted ultrasound signal. The mechanical index predicts the

cavitation activities during the ultrasound application at a particular combination of frequency and intensity. The mechanical index is preferably controlled by controlling the frequency and/or intensity of the emitted ultrasound signal.

[0094] In an embodiment of the invention, the emitted ultrasound signal has a spatial average temporal average intensity of less than 4 W/cm^2 . It is preferred that the intensity is in the range between 0.005 W/cm^2 and 1 W/cm^2 .

[0095] The controller 302, the signal generator and/or amplifier 301, and the ultrasound transducer 202 are also referred to as ultrasound device.

[0096] The display and control unit 400, as shown in Figure 1, preferably further comprises display means and input means. The display and control unit 400 is operationally connected to the ultrasound device and the information sending and/or receiving unit 203 via connection means 501, 503, 504. The connection means comprise a cable and/or a wireless connection.

[0097] In an embodiment of the invention the display and control unit 400 is preferably implemented as an application on a tablet computer, a desktop computer, and a smart phone. Alternatively the display and control unit 400 is designed as a stand alone device optionally comprising a battery.

[0098] Figure 4 shows a perspective view of one embodiment of an application head 205 of the system. The application head 205 is configured to accommodate the ultrasound transducer 202. Additionally and/or optionally the application head 205 is further configured to allow mechanical coupling and ultrasound coupling of the drug applicator 201 to the ultrasound transducer 202. The outer appearance of the application head 205 is preferably defined by an external housing. The external housing preferably comprises a first housing part 205a and a second housing part 205b.

[0099] Figure 5 shows a perspective view of one embodiment of the system according to one aspect of the invention. The system comprises the application head 205, the drug applicator 201, and additional housing and holding parts 700a. The additional housing and holding parts preferably accommodate all components of the system. Alternatively, some components of the system are accommodated in the at least one further housing (not shown). The additional housing and holding parts 700a are preferably configured to receive a patient's head. To receive a patient's head preferably a chin-rest and/or forehead-rest are provided. In one embodiment of the invention the application head 205 is attached to a flexible arm, allowing for an adjustment of the application head 205 and the drug applicator 201 relatively to the rest of the additional housing and holding parts 700a.

[0100] Figures 6 and 7 shows an alternative embodiment of the invention, wherein the application head and the system are integrated into a device that resembles the outer appearance of a pair of glasses. Directions such as front, left, and right are derived from directions during normal use of a glasses device. The application head 205 is preferably

formed in a front portion of the glasses device. The drug applicator 201 is preferably attached to the application head 205 at a position in front of the left and/or right eye. Further housing and holding parts 700b are preferably forming a frame and/or yokes of the glasses device. The advantage of the above design is the improved usability, especially the improved user experience during the application process.

[0101] Further embodiments of the invention relate to integration of the system according to one aspect of the invention into existing treatment apparatuses for diseases of the eye. The system is preferably combined and/or integrated with other diagnostic and/or treatment devices.

[0102] In one embodiment of the invention the system is operated in at least one application cycle. Each application cycle comprises at least one ultrasound emitting event with a time duration TA and a subsequent waiting period with a time duration TW. During the ultrasound emitting event the ultrasound device is operated and during the waiting period the ultrasound device is not operated. The drug applicator 201 is in contact with the scleral surface for the complete duration of the at least one application cycle.

[0103] Depending on the physical, chemical, and pharmaceutical properties of the drug different parameters for the application cycle are required. In one embodiment of the invention the system is configured to control at least one parameter, preferably a subset, selected from the following list: the time duration TA of the ultrasound emitting event, the time duration TW of the wait period after the ultrasound emitting event, the number of application cycles, the intensity of the ultrasound emitting event, the central frequency of the ultrasound emitting event, the mechanical index of the ultrasound emitting system, and in case of a pulsed ultrasound emitting event: the repetition rate of the ultrasound emitting event and the duty cycle of the ultrasound emitting event.

[0104] The size of the molecules comprising the drug to be delivered is of major importance for the parameters of the application cycle. For relatively small molecules, i.e., preferably having a size of less than 70 kDa, the drug delivery rate is primarily controlled by the duration of the ultrasound emission event TA. For relatively large molecules, i.e., preferably having a size of more than 70 kDa, the drug delivery rate is primarily controlled by the duration of the wait time TW after the ultrasound emission event.

[0105] Since the optimal set of parameters of the application cycle varies for different drugs and/or different users, in it is preferred that the system comprises means for assisting the setting of parameters of the application cycle. The means for assisting preferably use the information sending and/or receiving unit 203 to retrieve information about the drug from the drug applicator 201. The means for assisting preferably further use the display and input unit 400 to allow for changing of preset parameters.

[0106] In an embodiment of the invention, the system is connected to a central database and the database manages information about optimal sets of parameters of the application cycle.

Alternatively or additionally, optimal sets of parameters of the application cycle are stored on/in the drug applicator and are preferably retrieved by the information sending and/or receiving unit 203.

[0107] In an embodiment of the invention, the system comprises input means configured to manually set the parameters of the application cycle.

[0108] The system according to one aspect of the invention is configured to carry out the method according other aspects of the invention. In the following aspects of preferred embodiments of the method for ultrasound enhanced transscleral delivery of drugs are described. The skilled person realizes that certain above described embodiments of the system relate to certain embodiments of the method described hereinafter.

[0109] In an embodiment of the invention, the drug to be delivered is stored in the drug applicator 201. Prior to the delivery operation the drug applicator 201 is coupled to the application head 205. Prior to the coupling, a used drug applicator 201 is required to be removed. Prior or after the coupling the drug applicator 201 is prepared for the delivery operation. Preparing for the delivery operation preferably comprises removing a peel-off seal and/or removing a protective cover.

[0110] In an alternative embodiment, the drug is stored in a container holding several doses of the drug. A drug applicator 201 is preferably permanently coupled to the application head 202 and/or a drug applicator 201 is realisably coupled to the application head 202. The drug applicator 201 is optionally cleaned prior to loading the drug into the drug applicator 201. After the optional cleaning the drug is loaded into a drug receiving space 800 in the drug applicator 201. The loading can be carried out while the drug applicator 201 is attached to the application head 205 or while the drug applicator 201 is not attached to the application head 205.

[0111] In an embodiment of the invention, after the drug applicator 201 has been prepared for the delivery operation the system is prepared for the delivery operation. In an alternative embodiment of the invention the system is prepared for the delivery operation prior to preparing the drug applicator 201 for the delivery operation. Preparing the system for the delivery operation preferably comprises setting the optimal set of parameters of the application cycle and/or adapting the parameters of the application cycle. Prior to setting and/or adapting the parameters of the application cycle information about the drug and/or information about the drug applicator 201 are preferably retrieved by the information sending and/or receiving unit 203.

[0112] In an embodiment of the invention, after the system and/or the drug applicator 201 have been prepared for the delivery process the system is positioned such that the drug applicator touches the scleral surface. In an alternative embodiment, the system is positioned prior to preparing the system and/or the drug applicator.

[0113] Positioning the system preferably comprises applying an ultrasound transmission gel to

an interface 601b between the drug applicator 201 and the scleral surface. Positioning the system alternatively or additionally comprises pressing the drug applicator 201 against the scleral surface.

[0114] In an embodiment of the invention, after the system has been positioned the at least one application cycle is performed. During the application cycle the drug applicator 201 is in permanent contact with the sclera surface.

[0115] In an embodiment of the invention, during the at least one application cycle the temperature of the sclera surface is measured this measurement means. Measurement means preferably include a thermocouple and/or an infrared thermometer. It is preferred that the temperature of the scleral surface does not increase by more than 1°C during the at least one application cycle. The system is preferably configured to control the ultrasound emission event to prevent excessive heating of the scleral tissue.

[0116] In an embodiment of the invention, after the at least one application cycle and additional wait time is required for the drug to be delivered most efficiently.

[0117] In an embodiment of the invention after the at least one application cycle the drug applicator 201 is removed from the scleral surface. Depending on the embodiment of the invention the drug applicator 201 is preferably configured to be reused at a later time or is configured to be a single use drug applicator 201. Depending on the embodiment of the invention the drug applicator 201 is removed from the application head 205 after the at least one application cycle and/or remain on the application head 205 for later use.

[0118] The term "drug", as used herein, means a pharmaceutical formulation containing at least one pharmaceutically active compound. In one embodiment of the invention the pharmaceutically active compound has a molecular weight up to 70kDa and/or comprises antibodies, biologics conjugates, protein drug conjugates, corticosteroid drug conjugates, drug-encapsulated nanoparticles, drug-conjugated nanoparticles, protein drugs, biologics, corticosteroid drugs, nonsteroidal anti-inflammatory drugs, charged molecules, uncharged molecules, or a mixture of the above-mentioned pharmaceutically active compounds. In an alternative embodiment of the invention the pharmaceutically active compound has a molecular weight of more than 70kDa and/or comprises antibodies, biologics conjugates, protein drug conjugates, corticosteroid drug conjugates, drug-encapsulated nanoparticles, drug-conjugated nanoparticles, protein drugs, biologics, corticosteroid drugs, nonsteroidal anti-inflammatory drugs, charged molecules, uncharged molecules, or a mixture of the above-mentioned pharmaceutically active compounds.

[0119] In an embodiment the pharmaceutically active compound is useful for the treatment and/or prophylaxis of central retinal vein occlusion, branch retinal vein occlusion, central serous retinopathy, cytomegalovirus retinitis, retinoblastoma, intraocular lymphoma, ocular melanoma, giant cell arteritis, histoplasmosis, ischemic optic neuropathy, macular pucker, macular telangiectasia, uveitis, choroidal neovascularization, age-related macular

degeneration, diabetic retinopathy, glaucoma, retinitis pigmentosa, macular edema, macular degeneration, multirecurrent pterygia, ocular toxoplasmosis, proliferative vitreoretinopathy (PVR), Stevens-Johnson syndrome, ocular cicatricial pemphigoid, an ocular degenerative condition, or a post-surgery condition which requires the delivery of a drug into an intrascleral space.

[0120] The scope of protection of the invention is not limited to the examples given hereinabove. The invention is embodied in each novel characteristic and each combination of characteristics, which particularly includes every combination of any features which are stated in the claims.

REFERENCES CITED IN THE DESCRIPTION

Cited references

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Patent documents cited in the description

- [US20080177220A1](#) **[0006]**
- [US20100226971A1](#) **[0007]**
- [US5016615A](#) **[0008]**

Patentkrav

- 5 1. Lægemiddelapplikator (201) til et system til ultralydsforstærket transskleral levering af mindst ét lægemiddel til et målsted i et intraokulært rum (1), hvor systemet omfatter en signalgenererende enhed (300), der er operationelt forbundet med en ultralydstransducer (202),
hvor lægemiddelapplikatoren (201):
- i) omfatter mindst ét rum (800), der er konfigureret til at holde lægemidlet,
 - ii) er fremstillet af et materiale med lav ultralydsdæmpning med en ultralydsdæmpning på mindre end 10dB/(MHz cm),
 - 10 iii) er dannet af et blødt og elastisk materiale og konfigureret til at give mindre end 10% ultralydtabskobling af systemet til sklera, og
 - iv) er konfigureret til at blive mekanisk koblet til systemet og yderligere konfigureret til at blive koblet med en mekanisk kobling til ultralydstransduceren
 - 15 (202) med et ultralydstab på mindre end 20%; og
- hvor ultralydstransduceren (202) er konfigureret til at udsende en ultralydsbølgeform i mindst én påføringscyklus, hvor påføringscyklussen omfatter mindst én ultralydsudsendende hændelse med en varighed TA og en venteperiode med en varighed TW,
- 20 hvor det mindst ene rum (800) har mindst en åbning ved en overflade, der er beregnet til kobling med sklera.
- 25 2. Leveringsenhed (200) til et system til ultralydsforstærket transskleral levering af mindst ét lægemiddel til et målsted i et intraokulært rum (1), omfattende en lægemiddelapplikator (201) ifølge krav 1 og ultralydstransduceren (202).
- 30 3. System til ultralydsforstærket transskleral levering af mindst ét lægemiddel til et målsted i et intraokulært rum (1), hvilket system omfatter en signalgenererende enhed (300), der er operationelt forbundet til en ultralydstransducer (202) og en lægemiddelapplikator (201) ifølge krav 1.

4. Applikator ifølge krav 1 eller leveringsenheden ifølge krav 2 eller systemet ifølge krav 3, hvor lægemiddelapplikatoren (201) er konfigureret til at være udskiftelig og/eller udformet til en engangsanvendelse.

5 **5.** Applikatoren ifølge krav 1 eller 4 eller leveringsenheden ifølge krav 2 eller 4 eller systemet ifølge krav 3 eller 4, hvor lægemiddelmodtagelsesrummet (800) er forseglet ved overfladen, der er beregnet til kobling med sklera (601b), og forseglingen er konfigureret til at tillade lægemiddelgennemtrængning.

10 **6.** Applikator ifølge et hvilket som helst af kravene 1 og 4 til 5 eller leveringsenheden ifølge et hvilket som helst af kravene 2 og 4 til 5 eller systemet ifølge et hvilket som helst af kravene 3 til 5, hvor lægemiddelapplikatoren (201) er konfigureret til at blive fyldt og/eller genopfyldt, og hvor lægemiddelapplikatoren modtager mellem 10 µL og 1 ml af lægemidlet og eventuelt mindst en
15 yderligere substans.

7. Applikator ifølge et hvilket som helst af kravene 1 og 4 til 6 eller leveringsenheden ifølge et hvilket som helst af kravene 2 og 4 til 6 eller systemet ifølge et hvilket som helst af kravene 3 til 6, hvor lægemiddelapplikatoren (201) er
20 fremstillet fra et elastisk materiale med Youngs modul på mindre end 10 GPa.

8. Applikator ifølge et hvilket som helst af kravene 1 og 4 til 7 eller leveringsenheden ifølge et hvilket som helst af kravene 2 og 4 til 7 eller systemet ifølge et hvilket som helst af kravene 3 til 7, hvor lægemiddelapplikatoren (201) er
25 fremstillet fra mindst et af følgende materialer:

epoxyharpiks, polyurethangummi, polycarbonat, nylon 6 - 6, polyvinylchlorid, polyester, polyethylen med ultrahøj molekylvægt, polypropylen, teflon, polystyren, neoprengummi, polyvinylalkohol, polydimethylsiloxan, silikoneholdigt gummi, silikonehydrogel, silikonegummi, og

siliciumgummi doteret med mindst et af følgende materialer: nikkel, sølv, palladium, wolfram, guld, platin, siliciumoxid, titaniumoxid, aluminiumoxid, bariumsulfat, jernoxid, zirconiumdioxid, ceriumoxid, vismutoxid, ytterbiumoxid, lutetiumoxid, hafniumoxid.

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9. Applikator ifølge et hvilket som helst af kravene 1 og 4 til 8 eller leveringsenheden ifølge et hvilket som helst af kravene 2 og 4 til 8 eller systemet ifølge et hvilket som helst af kravene 3 til 8, yderligere omfattende en styreenhed (302), hvor styreenheden (302) er konfigureret til at styre mindst én af en flerhed af parametre i applikationscyklussen, hvor flerheden af parametre i applikationscyklussen er valgt blandt følgende:

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- a) varigheden TA for den ultralydsudsændende hændelse,
- b) varigheden TW af venteperioden efter den ultralydsudsændende hændelse,
- c) antallet af anvendelsescyklusser,
- d) intensiteten af den ultralydsudsændende hændelse,
- e) den centrale frekvens af den ultralydsudsændende hændelse,
- f) det mekaniske indeks for det ultralydsudsændende system, og i tilfælde af en pulserende ultralydsudsændende hændelse:
- g) gentagelseshastigheden af den ultralydsudsændende hændelse og
- h) driftscyklussen for den ultralydsudsændende hændelse.

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10. System ifølge krav 9, yderligere omfattende en informationsmodtagende og/eller -afsændende enhed (203),

hvor den informationsmodtagende og/eller -afsændende enhed (203) er konfigureret til at modtage og/eller sende en information relateret til lægemidlet; og hvor den informationsmodtagende og/eller -afsændende enhed (203) er operationelt forbundet til den signalgenererende enhed (300) og/eller styreenheden (302), eller hvor informationsmodtagende og/eller -afsændende enhed (203) er operationelt forbundet med den signalgenererende enhed (300) og/eller styreenheden (302), og styreenheden (302) er konfigureret til at styre

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mindst én af flerheden af parametre i applikationscyklussen baseret på informationen relateret til lægemidlet.

5 **11.** System ifølge krav 10, hvor informationen relateret til lægemidlet er lagret på lægemiddelapplikatoren (201).

10 **12.** System ifølge et hvilket som helst af kravene 10 til 11, hvor, når informationen relateret til lægemidlet inkluderer, at lægemidlet omfatter molekyler med en størrelse på 70 kDa eller mindre, er styreenheden (302) konfigureret til at styre varigheden TA til at være mellem 30 s og 300 s, og lægemiddelapplikatoren (201) er konfigureret således, at lægemidlet passerer gennem sklera i løbet af tidsperioden TA; og/eller
15 når informationen relateret til lægemidlet inkluderer, at lægemidlet omfatter molekyler med en størrelse på mere end 70 kDa, er styreenheden (302) konfigureret til at styre varigheden TW til at være mellem 60 s og 600 s, og lægemiddelapplikatoren (201) er konfigureret således, at lægemidlets molekyler passerer gennem sklera i løbet af tidsperioden TW.

20 **13.** System ifølge et hvilket som helst af kravene 9 til 12, hvor systemet yderligere omfatter en display- og/eller manuel inputenhed (400), der er konfigureret til at vise og/eller manuelt indstille mindst én af flerheden af parametrene i applikationscyklussen.

25 **14.** System ifølge et hvilket som helst af kravene 9 til 13, hvor systemet yderligere omfatter en temperatursensor, der er konfigureret til at registrere temperaturen på overfladen af sklera, og hvor styreenheden (302) er konfigureret til at styre ultralydsemissionsbegivenheden, således at under tid TA stiger temperaturen af overfladen af sklera ikke med mere end 1°C.

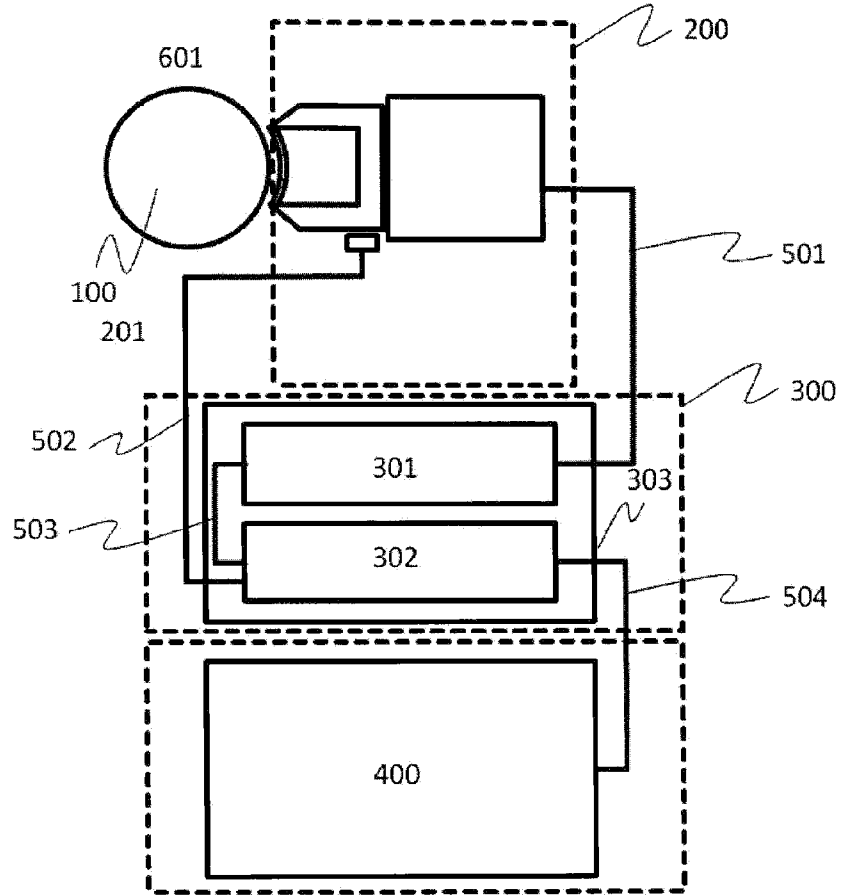
30

15. System ifølge krav 14, hvor temperatursensoren er et termoelement og/eller et infrarødt termometer.

DRAWINGS

18. Mai 2016

Fig. 1



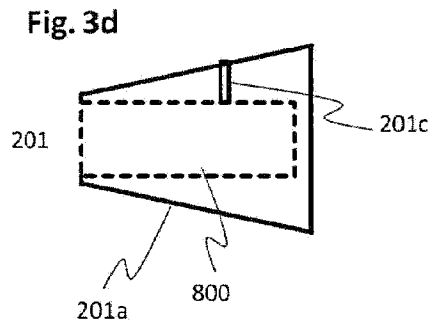
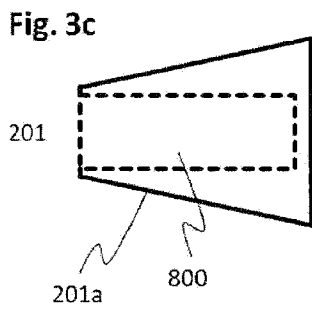
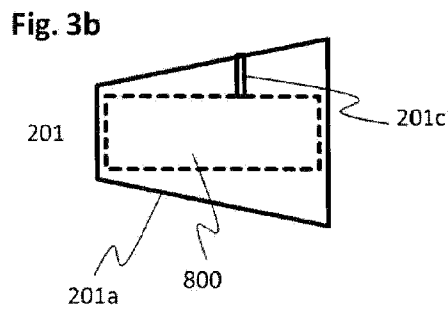
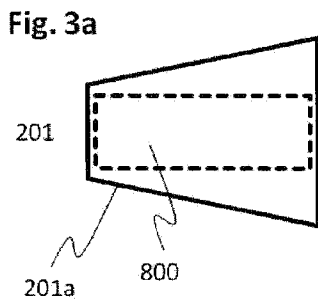
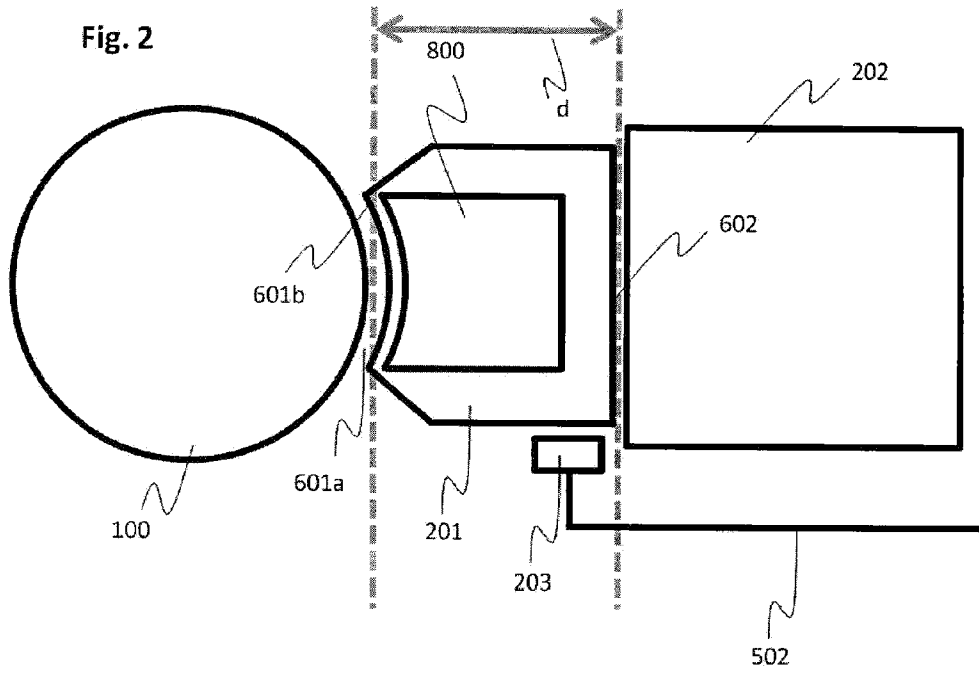


Fig. 4

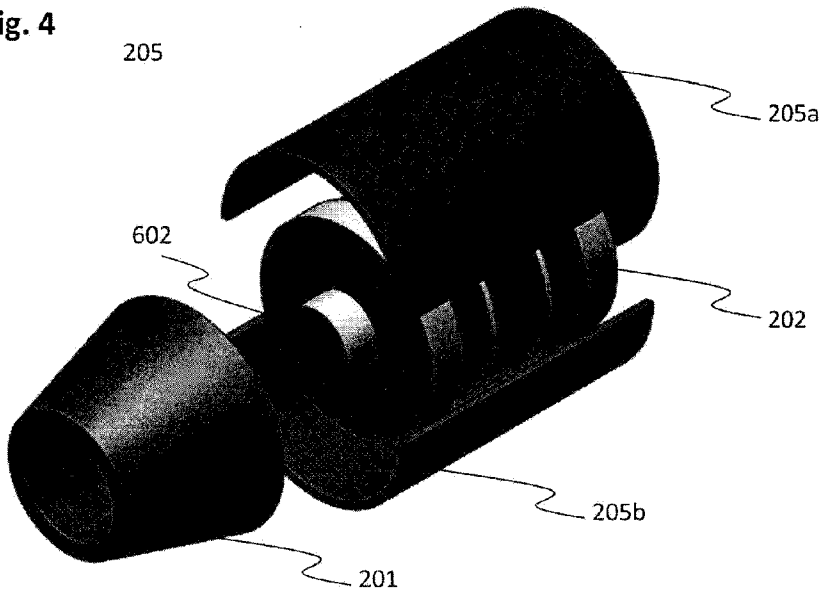


Fig. 5

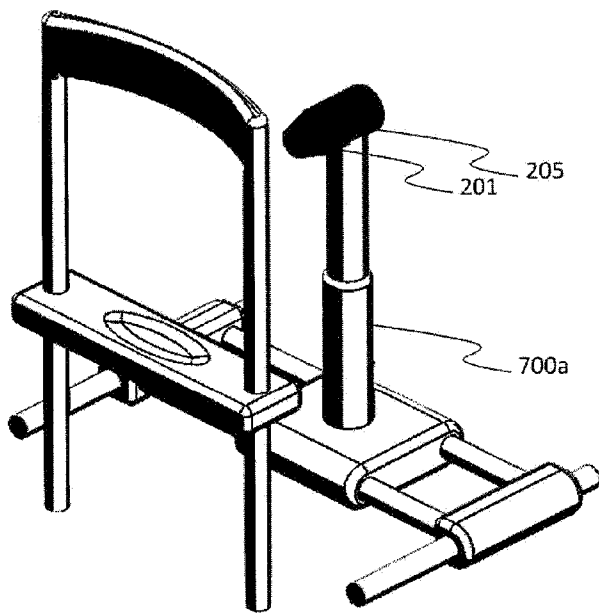


Fig. 6

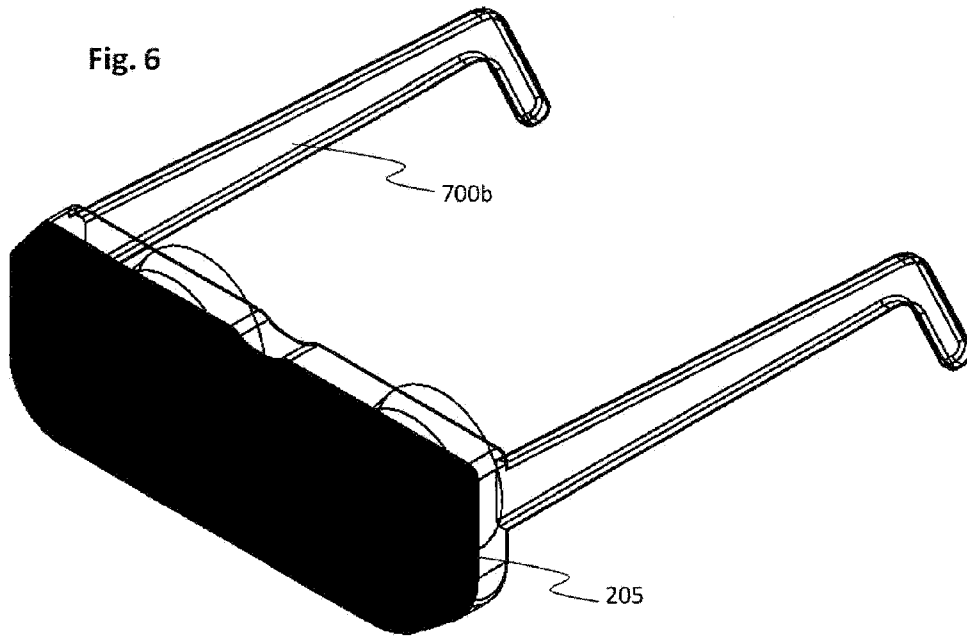


Fig. 7

