



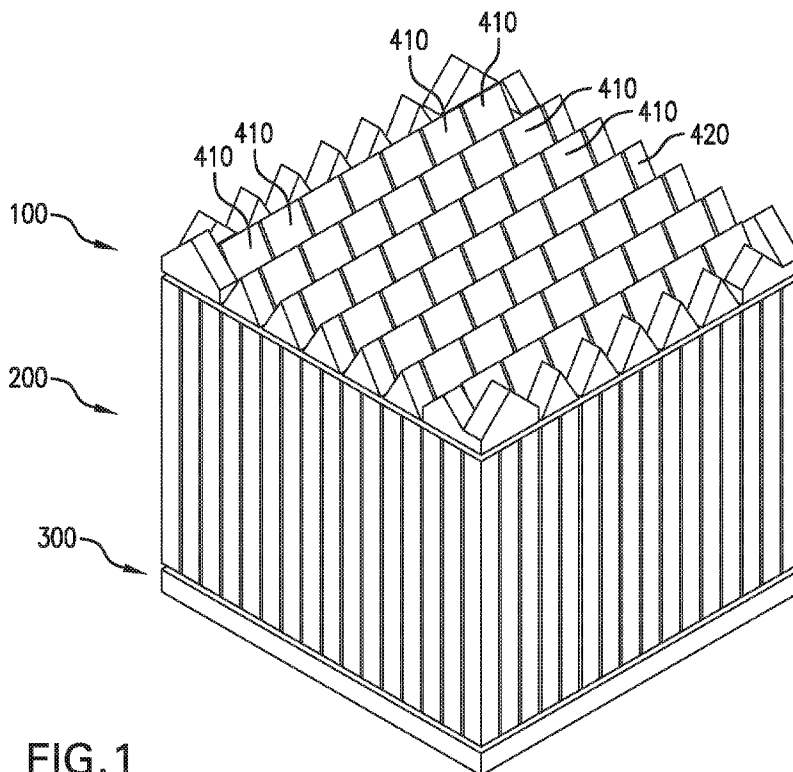
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(57) Abrégé/Abstract:

Provided are a device for detecting sub-atomic particles and method of fabrication thereof. The device includes a plurality of scintillators, a detector provided on a first end of the plurality of scintillators and a prismatoid provided on a second end of the plurality of scintillators. The prismatoid redirects light between adjacent scintillators of the plurality of scintillators.

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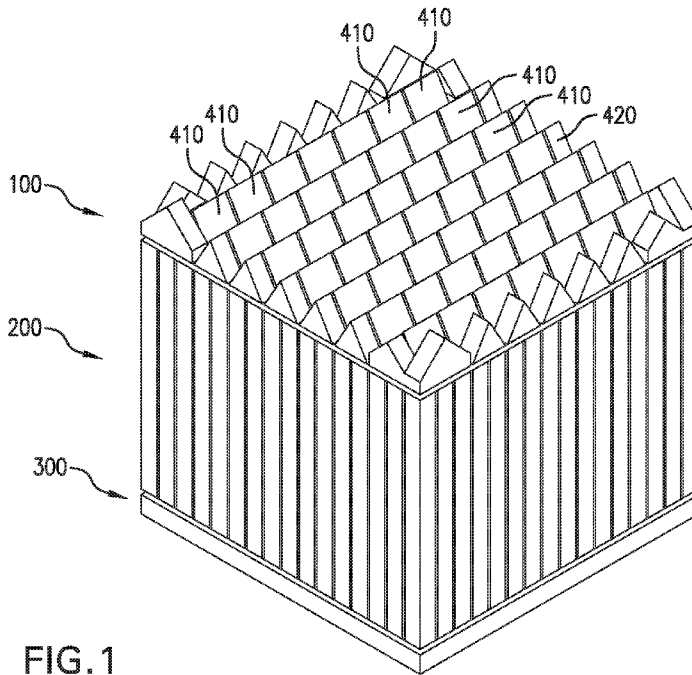


FIG. 1

(57) Abstract: Provided are a device for detecting sub-atomic particles and method of fabrication thereof. The device includes a plurality of scintillators, a detector provided on a first end of the plurality of scintillators and a prismatoid provided on a second end of the plurality of scintillators. The prismatoid redirects light between adjacent scintillators of the plurality of scintillators.



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## **PRISMATOID LIGHT GUIDE**

### **PRIORITY**

This application claims priority to U.S. Provisional Patent Applications No. 62/789,559 and 62/957,991 filed with the U.S. Patent and Trademark Office on January 8, 2019 and January 7, 2020, respectively, the entire contents of each which is incorporated herein by reference.

### **GOVERNMENT SUPPORT**

This invention was made with government support under grant number EB024849 awarded by the National Institutes of Health. The government has certain rights in the invention.

### **BACKGROUND OF THE INVENTION**

#### **1. Field of the Invention:**

The present invention relates generally to the field of radiation imaging and, in particular, to positron emission tomography (PET).

#### **2. Description of the Related Art:**

PET is a nuclear medical imaging modality that produces three-dimensional (3D) images to see functional processes in a living organism. PET is commonly used in clinical oncology for detecting cancer and for clinical diagnosis of heart problems and/or brain disorders. After being introduced into the organism, positron-emitting radionuclides decay with each annihilation, emitting two photons in diametrically opposing directions. Time of flight (TOF) measurements may be utilized to measure the time for the electromagnetic wave to travel a distance through a medium. A TOF PET system detects the photons, and uses TOF information to determine if two registered photons are in time coincidence, i.e., belong to a same positron annihilation event. The TOF PET system uses an arrival time difference to localize each annihilation event. Without the TOF localization data, computationally expensive iterative reconstruction algorithms are used to estimate the 3D distribution of events that provide the best match with the measured projection data. Modern PET readout is performed with silicon photomultipliers (SiPMs) due to their speed and magnetic resonance compatibility.

High depth-of-interaction (DOI) resolution is needed in PET scintillators to reduce parallax error and the resulting spatial blur, which is especially prominent in detection system with small ring diameters, such as single-organ inserts. DOI readout is traditionally performed with a double-sided readout using two readout arrays per scintillator array. However, the double-sided readout requires double electronics compared to a regular PET system. Therefore, recent research has focused on the development of single-sided readout techniques, which only requires one scintillator and one readout array. Multiple scintillator crystals are typically coupled to single readout pixels to reduce system cost, although 1:1 coupling can also be used.

Modern DOI techniques use substantially flat reflective light guides at the top of the scintillator array to redirect light to other readout pixels. In doing so, DOI information can be gained by detection of a fraction of the maximum light absorbed on a single SiPM pixel and the detected fraction to the total light absorbed across all pixels of an array for a single gamma ray interaction event. Only two different readout pixels are required to make this measurement. However, having more pixels is useful to improve the DOI resolution.

Conventional light guide geometry uses a flat, uniform reflective material, which primarily directs light back into the original scintillation crystal that gamma ray absorption took place in, rather than redirecting the light to other crystals and readout pixels. This results in suboptimal DOI resolution since most of the light is not being shared with other pixels, which is required to make DOI measurements, thus making single-sided DOI readout ineffective. Current single-sided DOI readout with high aspect ratio scintillators (~15-20mm thick) and uniform light guides are only able to achieve ~5mm full width at half maximum (FWHM) DOI resolution. In contrast, double-sided readout can achieve DOI resolution on the order of 1mm FWHM, leaving much room for improvement of single-sided techniques before they become feasible to use in practice. Conventional systems and methods fail to provide impactful light sharing techniques in PET detector systems.

Anger logic schemes are traditionally employed to improve the overall detector system resolution by localizing gamma ray interaction down to the crystal level via centroiding. Because of poor light sharing of conventional uniform light guides, Anger logic localization on the periphery of the detector array is severely degraded compared to that of centralized crystals and detectors since peripheral crystals have fewer crystals and pixels for sharing.

## SUMMARY OF THE INVENTION

To overcome shortcomings of conventional systems, provided herein are a system and method for improved light sharing between scintillator crystals in PET detector systems. The present disclosure overcomes the shortcomings of conventional DOI readout systems and methods, provides improved DOI resolution and more uniform Anger logic localization performance across entire detector arrays.

Accordingly, aspects of the present invention address the above problems and disadvantages and provide the advantages described below. An aspect of the present invention provides a device for detecting sub-atomic particles, the device including a plurality of scintillators, at least one detector provided on a first end of the scintillator, and a prismaoid provided on a second end of the scintillator, with the prismaoid configured to redirect light between a first pair of adjacent scintillators of the plurality of scintillators.

An aspect of the present disclosure provides a prismaoid that includes a reflective surface configured to redirect travel of at least one photon emitted from at least one scintillator of a pair of scintillators adjacent to the reflective surface, with the travel of the at least one photon being redirected from the at least one scintillator of a first pair of scintillators toward another scintillator of the first pair of scintillators.

A further aspect of the present disclosure provides a system for non-invasive medical imaging that includes at least one prismaoid, at least one detector, and a scintillator array. The at least one prismaoid redirects light between adjacent scintillators of scintillator array. The at least one detector is provided on an end of the scintillator array opposite the at least one prismaoid, and the prismaoid is substantially shaped as at least one of at least one prism, at least one antiprism, at least one frustum, at least one triangle, at least one cupola, at least one parallelepiped, at least one wedge, at least one pyramid, at least one truncated pyramid, and at least one portion of a sphere.

## BRIEF DESCRIPTION OF THE DRAWINGS

The above and other aspects, features and advantages of certain embodiments of the present invention will be more apparent from the following detailed description taken in conjunction with the accompanying drawings, in which:

FIG. 1 is a perspective view of the prismaoid light guide, according to an embodiment of the present disclosure;

FIG. 2 is a perspective view of a prismatic light guide, according to an embodiment of the present disclosure;

FIG. 3 is a cut away profile view of a prismatic light guide positioned on a scintillator array, according to an embodiment of the present disclosure;

FIG. 4 is a top view of a prismatic light guide, according to an embodiment of the present disclosure;

FIGs. 5a-5c are perspective views of prisms, according to embodiments of the present disclosure;

FIG. 6 is a perspective view of a second prism, according to an embodiment of the present disclosure;

FIGs. 7a and 7b are perspective views of prisms, according to embodiments of the present disclosure;

FIG. 8a illustrates a prismatic light guide array disassembled from a scintillator array, according to an embodiment of the present disclosure;

FIG. 8b illustrates a scintillator array disassembled from a prismatic light guide array, according to an embodiment of the present disclosure;

FIG. 9(a) illustrates light sharing of a conventional planar light guide;

FIG. 9(b) illustrates light sharing of a prism, according to an embodiment of the present disclosure;

FIG. 10 provides simulated illuminance maps for a conventional planar light guide;

FIG. 11 provides simulated illuminance maps according to an embodiment of the present disclosure; and

FIG. 12 is a graph of percent light-sharing across neighboring silicon photomultiplier detectors comparing the percentage light sharing of conventional planar glass with the prismatic light guide according to an embodiment of the present disclosure.

## **DETAILED DESCRIPTION OF EMBODIMENTS OF THE INVENTION**

The following detailed description of certain embodiments of the present invention will be made with reference to the accompanying drawings. In describing the invention, explanation about related functions or constructions known in the art are omitted for the sake of clarity, to avoid obscuring the invention with unnecessary detail.

FIG. 1 is a perspective view of the prismatic light guide, according to an embodiment of the present disclosure. The prismatic light guide 100 of FIG. 1 is positioned on the scintillator array 200, with a detector 300 positioned on a side opposite the prismatic light guide 100. As illustrated in FIG. 1, the prismatic light guide 100 includes a plurality of first prisms 410, which may be triangular shaped, and which may be surrounded by second prisms 420 and corner prisms, details of which are provided herein. The prism light guide 100 may be fixedly provided or removably provided on the scintillator array 120.

FIG. 2 is a perspective view of the prismatic light guide 100. As illustrated in FIG. 2, the plurality of first prisms 410 may be substantially pyramid shaped. The first prisms 410, the second prisms 420 and the third prisms may be substantially shaped as at least one of at least one prism, at least one antiprism, at least one frustum, at least one triangle, at least one cupola, at least one parallelepiped, at least one wedge, at least one pyramid, at least one a truncated pyramid, and at least one a portion of a sphere.

FIG. 3 is a cut away profile view illustrating a geometric arrangement of a center portion of the prismatic light guide 100 positioned on a scintillator array 200, according to an embodiment of the present disclosure. As illustrated in FIG. 3, the prismatic light guide 100 may be substantially shaped as a pyramid with three sides 120a, 120b, 120c. The prismatic light guide 100 may be positioned on or adjacent to a first end 211d, i.e., a first end face, of the scintillator array 200. The prismatic light guide 100 operates as a reflector that enhances light sharing and provides at least 4:1 coupling between scintillators 211, 212, 213, 214. The prismatic light guide 100 includes at least one reflective surface, e.g., an interior surface of sides 120a, 120b, that redirects travel of at least one sub-atomic particle, e.g., a photon, emitted from at least one scintillator of a first pair of adjacent scintillators. The interior surface of sides 120a, 120b may be coated with Barium Sulfate, epoxy or provided with an enhanced specular reflector (ESR) insert for improved reflectivity along lateral face thereof. Each scintillator of the scintillator pair of scintillators may be a scintillator crystal, configured to convert high energy x-rays, gamma rays and similar high energy particles into optical light and/or photons, as known in the art. The change of travel direction is from the at least one scintillator that emits the at least one sub-atomic particle towards at least one other scintillator of the at least four adjacent scintillators. The provided coupling enhances detection by silicon photomultipliers (SiPM) pixels 380a, 380b, 380c...380i of detector 300, positioned at a second end 211b. The SiPM pixels 380a...380i of detector 300 communicate with at least one

processor, which controls a display or other output of the at least one photon that is detected by the detector 300, to provide a single-sided readout high resolution of depth-of-interaction (DOI) readout in a positron emission tomography (PET) detector.

Each scintillator 211, 212, 213, 214 may include a first interior side 211a, 212a and a second interior side 211c, 212c. The second interior side 211c, 212c may be substantially parallel with the respective first interior side 211a, 212a, and the first interior side 211a, 212a and the second interior side 211c, 212c run substantially from the first end 211d to the second end 211b, thereby providing an interior light guide 211g, 212g between each respective first side 211a, 212a and second side 211c, 212c configured to reflect light therebetween, for transmitting substantially all of the light from respective prisms 120 of the prism light guide 100 to respective detectors 300. The interior light guide reflects substantially all light within respective scintillators 211, 212, 213, 214 traveling from respective prisms 120 to respective detectors 300. As illustrated in FIG. 9B, the prism 120 redirects light from the light guide of a first scintillator to the light guide of adjacent scintillators, and light sharing is self-contained within scintillation crystals coupled to the prism 120.

The prism 120 provides stabilized light guide geometry at the first end face 211d of the scintillator array 100. The prism light guide 100 reflects light, without functioning as a high-energy photon detector. As illustrated in FIGs. 3, 4, 8a and 8b, the scintillators 211, 212, 213, 214 may be coupled in a 4:1 ratio for photon detection by a shared SiPM pixel, e.g., SiPM pixel 380a and SiPM pixel 380b being shared by scintillators 211, 212, 213, 214 via prism 120 of prism light guide 100.

At least two SiPM pixels 380a, 380b of the detector 300 are coupled to a respective prism 120 via scintillator crystals 211, 212, 213, 214, to enable differential single-sided readout for DOI capabilities. FIGs. 3, 4, 8a and 8b illustrate a 1:4 scintillator-to-readout coupling ratio. Prism 120 may be coupled to one end of crystals 211, 212, 213, 214, and SiPM pixels 380a, 380b may be coupled to an opposite end. Other coupling ratios can also be used with varied prism geometry, with the prism 120 being substantially shaped as at least one of at least one prism, at least one antiprism, at least one frustum, at least one triangle, at least one cupola, at least one parallelepiped, at least one wedge, at least one pyramid, at least one a truncated pyramid, and at least one a portion of a sphere.

FIG. 4 is a top view of the prismatic light guide 100, with locations of varied prismatic geometries to introduce more uniformly directed light sharing along edges of the scintillator array 200. The geometry of the prismatic array allows for coupling of each non-peripheral prismatic to four SiPM pixels of detector 300 and improved controlled light sharing. FIG. 4 illustrates scintillators 211, 212, 213, 214 sharing a common detector 300. Scintillators 211 and 212 may also be provided as a first pair of adjacent scintillators, and scintillators 213, 214 may be provided as a second pair of adjacent scintillators, with the first scintillator of the first pair of adjacent scintillators adjacent to a first scintillator of the second pair of adjacent scintillators, and the first scintillator of the first pair of adjacent scintillators sharing a first detector of a plurality of detectors with the first scintillator of the second pair of adjacent scintillators. The second scintillator of the first pair of adjacent scintillators may be adjacent to a second scintillator of the second pair of adjacent scintillators, and the second scintillator of the first pair of adjacent scintillators may share a second detector of the plurality of detectors with the second scintillator of the second pair of adjacent scintillators. Accordingly, the prismatic may redirect light from the first scintillator of the first pair of adjacent scintillators to at least one of the second scintillator of the first pair of adjacent scintillators, the first scintillator of the second pair of adjacent scintillators, and the second scintillator of the second pair of adjacent scintillators.

The controlled light sharing of the present disclosure increases system-level count rate. In contrast, in a uniform light guide, each scintillation event requires readout from all SiPM pixels to calculate the DOI and perform centroiding, since light is expected to be shared across all scintillators. On the other hand, the prismatic light guide of the present disclosure provides precise identification of which scintillator columns will share light with each other. Scintillators will only share light with columns coupled to a same prismatic. As illustrated, each non-peripheral prismatic is coupled to at least four scintillators, which belong to anywhere from at least two to four SiPM pixels depending on the detector array geometry. As a result, readout is only required for a smaller subset of pixels at a time for each scintillation event, enabling simultaneous readout in other parts of the detector array, thereby increasing the system-level count rate when compared with the count rate of a detector system using a conventional uniform light guide.

FIGs. 5a-5c are perspective views of prismatoids, according to embodiments of the present disclosure. FIG. 5a is a perspective view of a first prismatoid 410 in a substantially pyramid shape.

FIG. 5b is a perspective view of a first prismatic 410 in shape that combines a substantially pyramid shape with a substantially cuboid shape. FIG. 5c is a perspective view of a first prismatic 410 in a substantially triangular shape.

FIG. 6 is a perspective view of a second prismatic 420. The second prismatic 420 has a substantially triangular shape.

FIGs. 7a and 7b are perspective views of prismatic 430. FIG. 7a illustrates a corner prismatic that includes substantially cuboid shapes 435, 436, upon which substantially triangular shapes 432, 433 are respectively affixed. The cuboid shapes 435, 436 may also be monolithically formed on triangular shapes 432, 433. FIG. 7b illustrates a corner prismatic that includes substantially cuboid shapes 430a, 430b, upon which substantially triangular shapes 430c, 430d are respectively affixed. Arrangement of the first prismatic 410, the second prismatic 420 and the third prismatic 430 is provided in FIGs. 2-4.

Increased uniformity of Anger logic centroiding resolution throughout the detector array is provided, since light is purposely directed to other pixels. In contrast, in conventional uniform light guides do not specifically couple or purposely direct light to specific other SiPM pixels. Also, conventional uniform light guides introduce edge effects where centroiding resolution decreases drastically along the edges of the scintillator array. In contrast, the configuration of the first prismatic 410, the second prismatic 420 and the third prismatic 430 is completely symmetrical regarding light sharing between scintillators and eliminates edge effects in conventional systems. See, FIGs. 2-4.

FIG. 8a illustrates a prismatic light guide array disassembled from a scintillator array, according to an embodiment of the present disclosure. FIG. 8b illustrates a scintillator array disassembled from a prismatic light guide array, according to an embodiment of the present disclosure. Assembly of the prismatic light guide array 100 of FIG. 8a onto the scintillator array 200 of FIG. 8b provides a 4:1 scintillator to prismatic ratio. The prismatic light guide array 100 and the scintillator array 200 may also be monolithically provided.

FIG. 9(a) illustrates light sharing of a conventional planar light guide. FIG. 9(b) illustrates light sharing of a prismatic light guide according to an embodiment of the present disclosure. FIGs. 9(a) and 9(b) are obtained by Monte Carlo simulation. FIGs. 9A and 9B provide flood histograms at the upper portion thereof and one dimensional histograms of gamma ray interaction localization in the x-direction representative of crystal identification quality at the lower portion

thereof. FIG. 9A illustrates non-uniform scintillator column identification with the uniform glass light guide using Anger logic centroiding due to edge and corner effects. FIG. 9b illustrates elimination of edge and corner effects due to improved light sharing patterns, thereby enabling uniform scintillator column identification throughout the detector array in accordance with an aspect of the present disclosure.

Comparison of the ray traces of FIG. 9(a) with the ray traces of FIG. 9(b) show improved sharing of light with neighboring scintillator column provided by prismatic light guide 100. As shown in FIG. 9(b), the prismatic redirects light into neighboring scintillators and SiPM pixels, thus enabling more accurate DOI readout due to enhanced light sharing between neighboring scintillators.

FIG. 10 provides simulated illuminance maps for a conventional planar light guide. FIG. 11 are simulated illuminance maps according to an embodiment of the present disclosure. The illuminance maps of FIGs. 10 and 11 are heatmaps of photon flux on respective SiPM pixels.

As shown in the conventional planar uniform light guide of FIG. 10, most light lands in a bottom right corner of the pixel corresponding to the scintillator where the gamma ray interaction took place. However, for DOI readout, a larger portion of the light would ideally be shared with neighboring pixels to gain more information on where exactly in the scintillator the interaction took place.

As shown in FIG. 11, using the same scintillator as in FIG. 10 but replacing the planar uniform light guide with the prismatic light guide 100, the light sharing of the gamma ray interaction takes is greatly enhanced with adjacent SiPM pixels, as well as the SiPM pixels diagonally across from the original readout pixel.

FIG. 12 is a graph of percent light-sharing across neighboring SiPM detectors comparing percentage light sharing of conventional planar glass with the prismatic light guide. As illustrated in FIG. 12, the prismatic light guide 100 provides significantly improved light sharing for all interaction depths, with the improvement increasing as a function of interaction depth, illustrating enhanced DOI localization accuracy, which in turn provides improved DOI resolution and spatial resolution of PET detector systems.

A method of fabrication is provided that includes affixing the prismatic light guide onto one end of a scintillator, which may be provided as a block of scintillator crystals, with the detector module affixed to an opposite end of the scintillator. The prismatic 120 may be deposited on the

one end of the scintillator array by sputtering. The prismatoid may also be removably attached to the one end of the scintillator. The scintillators may be polished and then de-polished along lateral faces thereof to introduce roughness and improve DOI resolution by creating differential light sharing along the lateral faces as a function of gamma ray interaction depth.

While the invention has been shown and described with reference to certain aspects thereof, it will be understood by those skilled in the art that various changes in form and details may be made therein without departing from the spirit and scope of the present invention as defined by the appended claims and equivalents thereof. No recitation of any claim set forth below is to be construed as a means plus function element without express use of “means for” or “step for.”

**WHAT IS CLAIMED IS:**

1. A device for detecting sub-atomic particles, the device comprising:  
a plurality of scintillators;  
at least one detector provided on a first end of the scintillator; and  
a prismaoid provided on a second end of the scintillator,  
wherein the prismaoid is configured to redirect light between a first pair of adjacent scintillators of the plurality of scintillators.
2. The device of claim 1, wherein the prismaoid comprises at least one reflective surface for redirecting travel of at least one sub-atomic particle emitted from at least one scintillator of the first pair of adjacent scintillators.
3. The device of claim 2, wherein the travel of the at least one sub-atomic particle is redirected from an emitting scintillator toward another scintillator of the first pair of adjacent scintillators.
4. The device of claim 1, wherein the prismaoid is substantially shaped as at least one of at least one prism, at least one antiprism, at least one frustum, at least one triangle, at least one cupola, at least one parallelepiped, at least one wedge, at least one pyramid, at least one truncated pyramid, and at least one portion of a sphere.
5. The device of claim 1, further comprising a second pair of adjacent scintillators,  
wherein a first scintillator of the first pair of adjacent scintillators is adjacent to a first scintillator of the second pair of adjacent scintillators, and  
wherein the first scintillator of the first pair of adjacent scintillators shares a first detector of the at least one detector with the first scintillator of the second pair of adjacent scintillators.
6. The device of claim 5, wherein a second scintillator of the first pair of adjacent scintillators is adjacent to a second scintillator of the second pair of adjacent scintillators, and

wherein the second scintillator of the first pair of adjacent scintillators shares a second detector of the at least one detector with the second scintillator of the second pair of adjacent scintillators.

7. The device of claim 6, wherein the prismaoid is configured to redirect light from the first scintillator of the first pair of adjacent scintillators to at least one of the second scintillator of the first pair of adjacent scintillators, the first scintillator of the second pair of adjacent scintillators, and the second scintillator of the second pair of adjacent scintillators.

8. The device of claim 1, wherein each scintillator of the first pair of adjacent scintillators comprises a first interior side and a second interior side substantially parallel with the first interior side.

9. The device of claim 8, wherein the first interior side and the second interior side are configured to reflect light therebetween, for transmitting substantially all of the light from the prismaoid to the at least one detector.

10. The device of claim 1, wherein the at least one detector comprises at least one pixilated sensor.

11. The device of claim 10, wherein the device further comprises at least one processor configured to communicate with the at least one pixilated sensor to perform positron emission tomography (PET) by sensing at least one photon.

12. An prismaoid comprising:  
a reflective surface configured to redirect travel of at least one photon emitted from at least one scintillator of a pair of scintillators adjacent to the reflective surface,  
wherein the travel of the at least one photon is redirected from the at least one scintillator of a first pair of scintillators toward another scintillator of the first pair of scintillators.

13. The prismaoid of claim 12, wherein at least one detector is provided on an end of the first pair of scintillators opposite the reflective surface, and

wherein a second pair of adjacent scintillators is provided with a first scintillator of the first pair of adjacent scintillators sharing a first detector of the at least one detector with a first scintillator of the second pair of adjacent scintillators.

14. The prismaoid of claim 13, wherein a second scintillator of the first pair of adjacent scintillators is adjacent to a second scintillator of the second pair of adjacent scintillators, and

wherein the second scintillator of the first pair of adjacent scintillators shares a second detector of the plurality of detectors with the second scintillator of the second pair of adjacent scintillators.

15. The prismaoid of claim 12, wherein the prismaoid is configured to redirect light from a first scintillator of the first pair of adjacent scintillators to at least one of a second scintillator of the first pair of adjacent scintillators, a first scintillator of the second pair of adjacent scintillators, and a second scintillator of the second pair of adjacent scintillators.

16. The prismaoid of claim 15, wherein each scintillator of at least two adjacent scintillators of the pair of scintillators comprises a first interior side and a second interior side substantially parallel with the first interior side, and

wherein the first interior side and the second interior side are configured to reflect light therebetween, for transmitting substantially all of the light from the prismaoid to at least one detector.

17. The prismaoid of claim 12, wherein the prismaoid is substantially shaped as at least one of at least one prism, at least one antiprism, at least one frustum, at least one triangle, at least one cupola, at least one parallelepiped, at least one wedge, at least one pyramid, at least one truncated pyramid, and at least one portion of a sphere.

18. A system for non-invasive medical imaging, the system comprising:  
at least one prismaoid;

at least one detector; and  
a scintillator array,  
wherein the at least one prismatic is configured to redirect light between adjacent scintillators of scintillator array,  
wherein the at least one detector is provided on an end of the scintillator array opposite the at least one prismatic, and  
wherein the at least one prismatic is substantially shaped as at least one of at least one prism, at least one antiprism, at least one frustum, at least one triangle, at least one cupola, at least one parallelepiped, at least one wedge, at least one pyramid, at least one truncated pyramid, and at least one portion of a sphere.

19. The system of claim 18, wherein the system is configured to perform positron emission tomography (PET) with a single-sided depth-of-interaction (DOI) readout having high coincidence time resolution (CTR) and high-count rate.

20. The system of claim 19, wherein the scintillator array, the at least one prismatic, and the at least one detector are asymmetrically aligned, and  
wherein a first detector of the at least one detector abuts a second detector of the at least one detector, to extend an area for performing the PET.

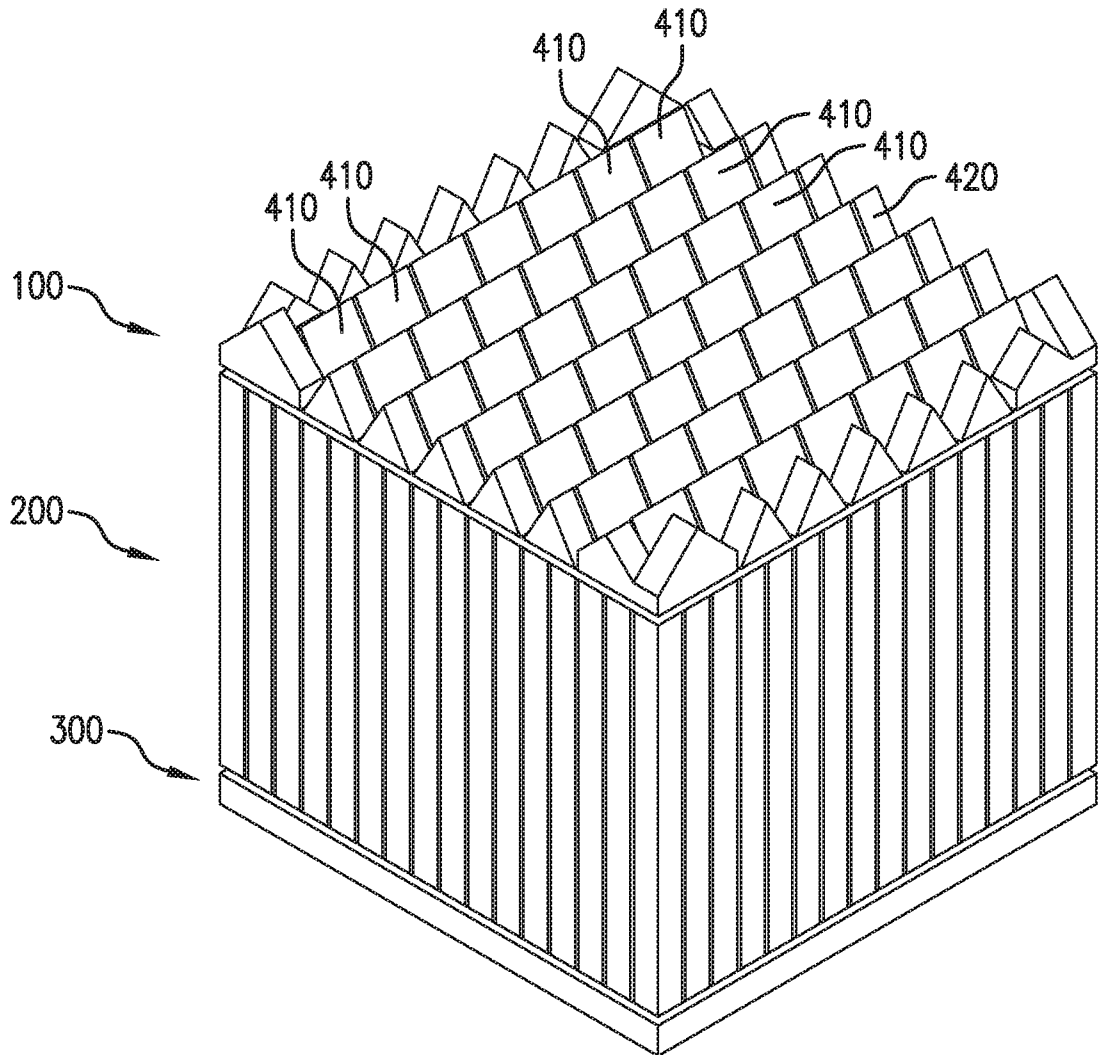


FIG. 1

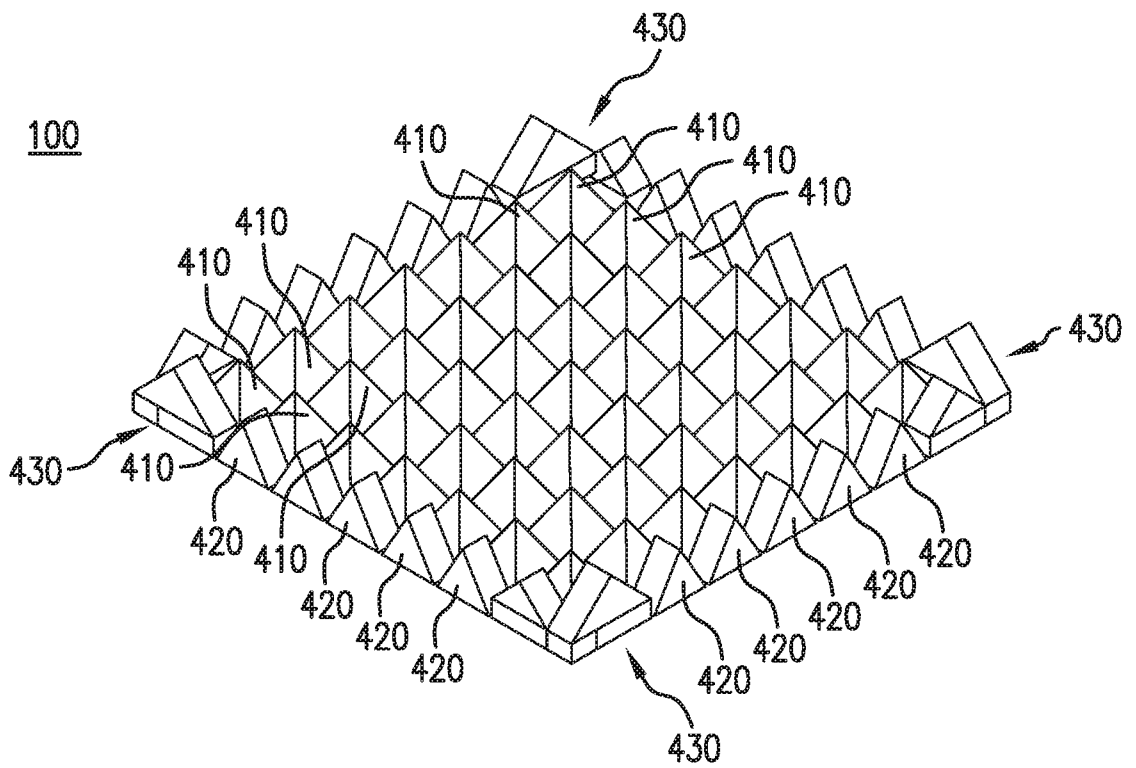


FIG. 2

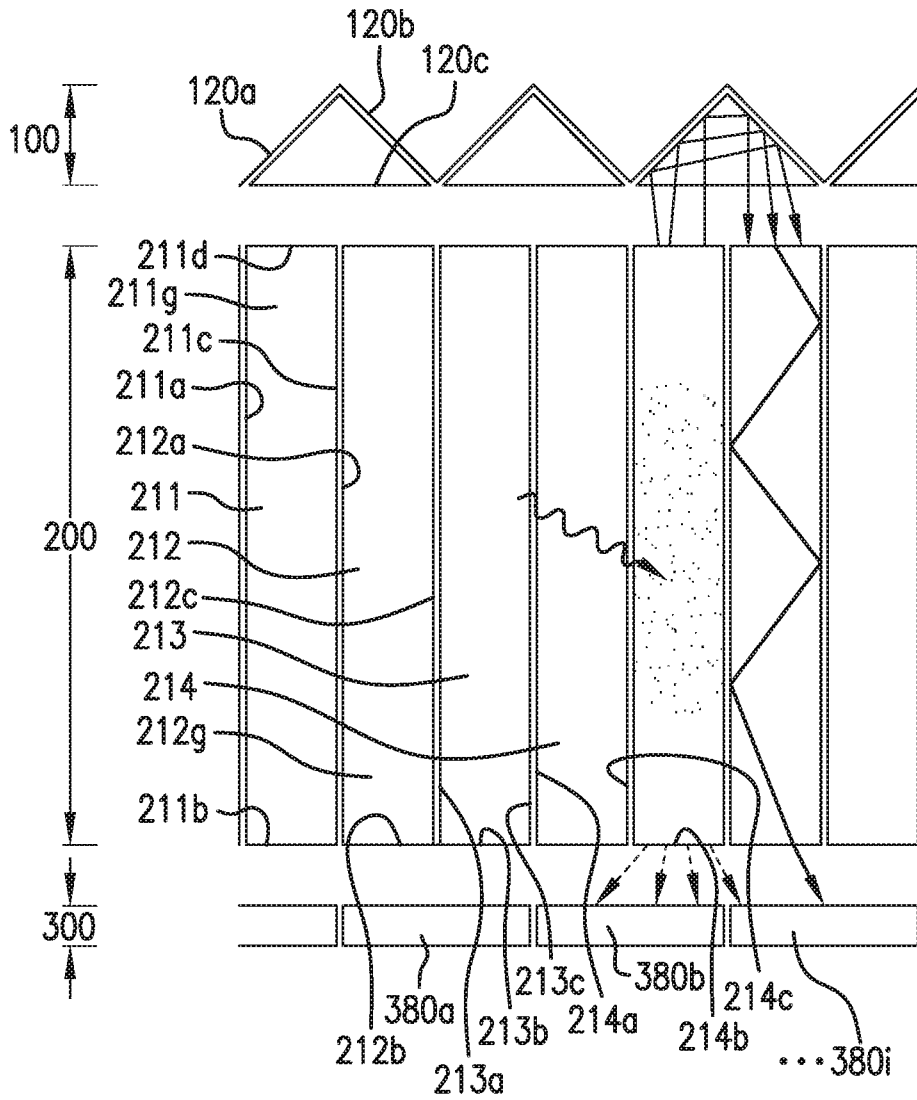


FIG. 3

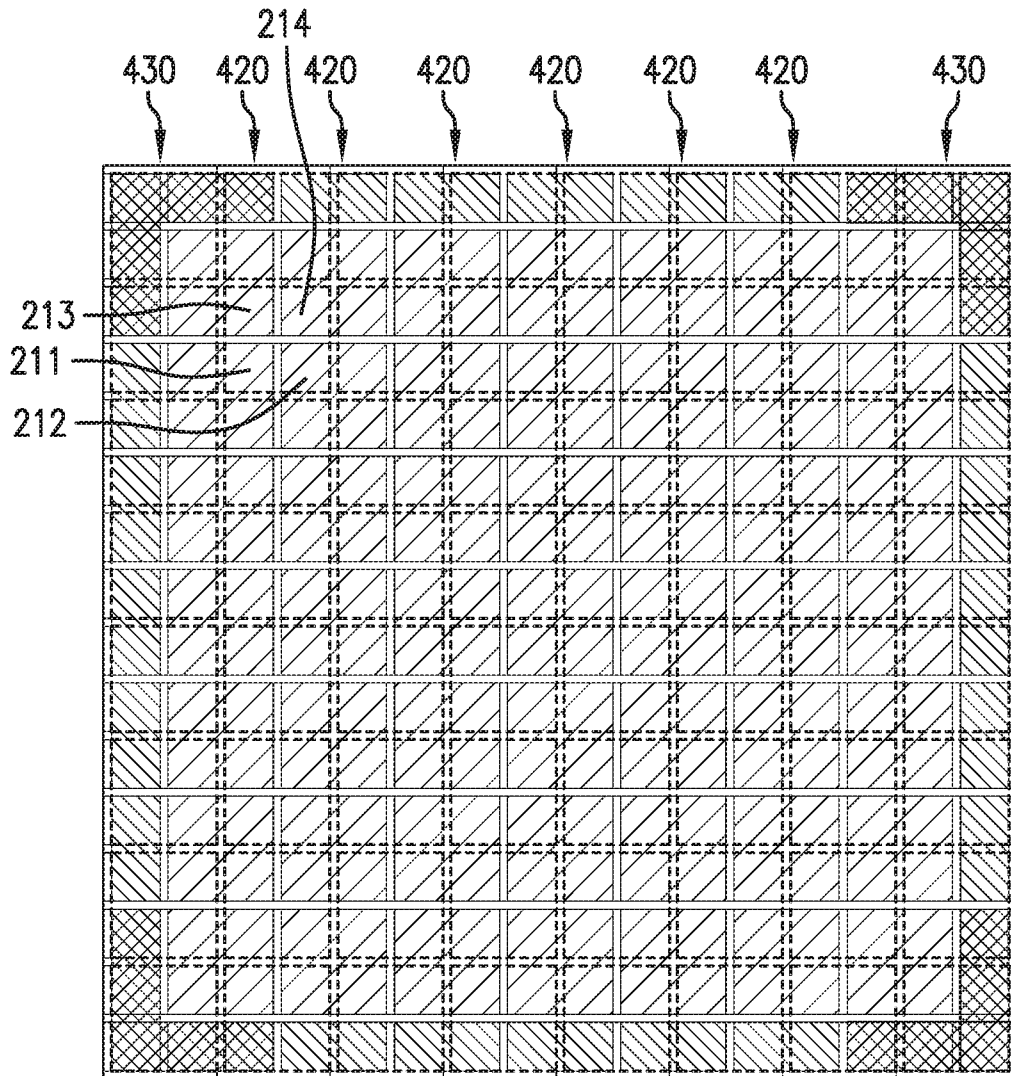


FIG.4

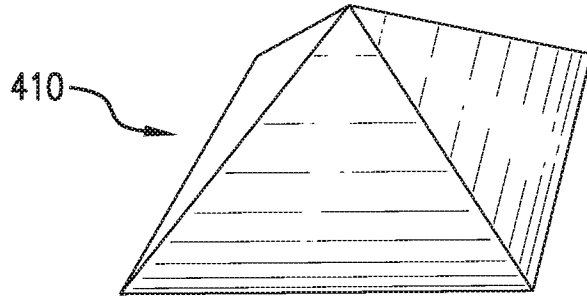


FIG. 5A

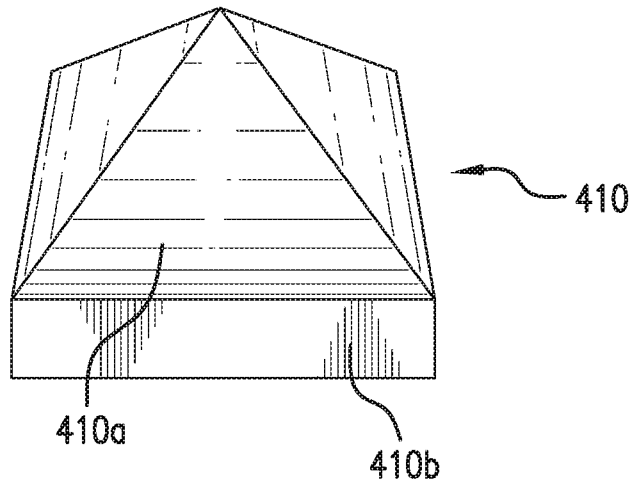


FIG. 5B

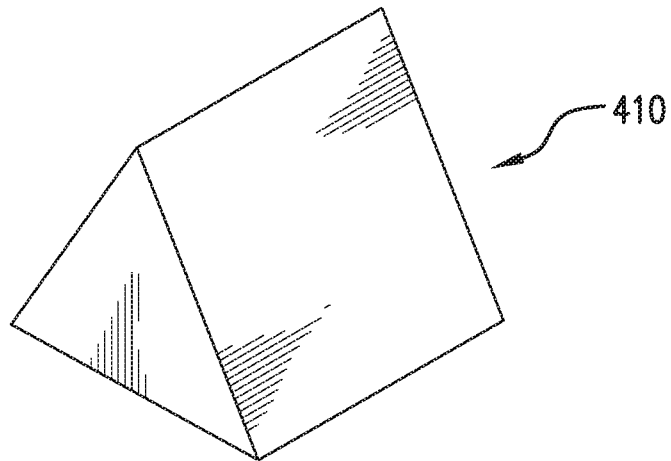


FIG. 5C

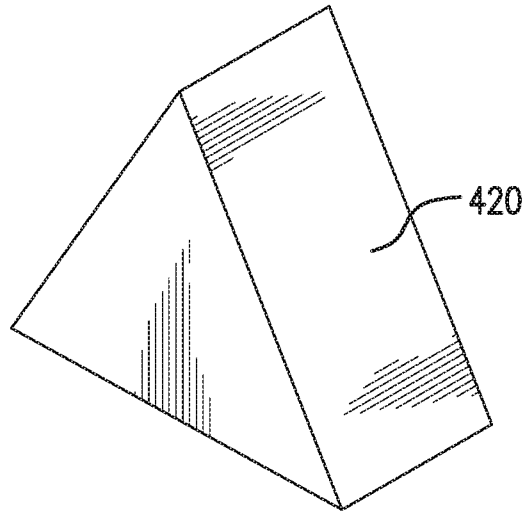


FIG. 6

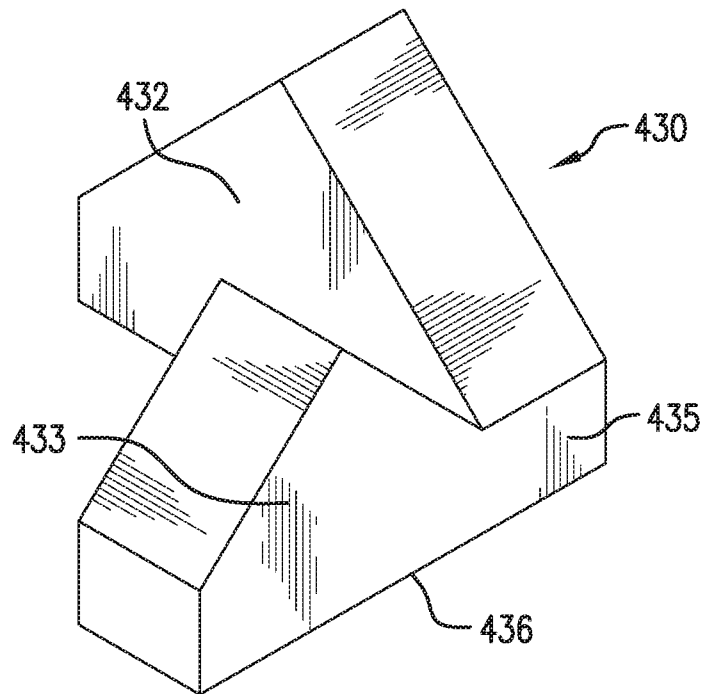


FIG. 7A

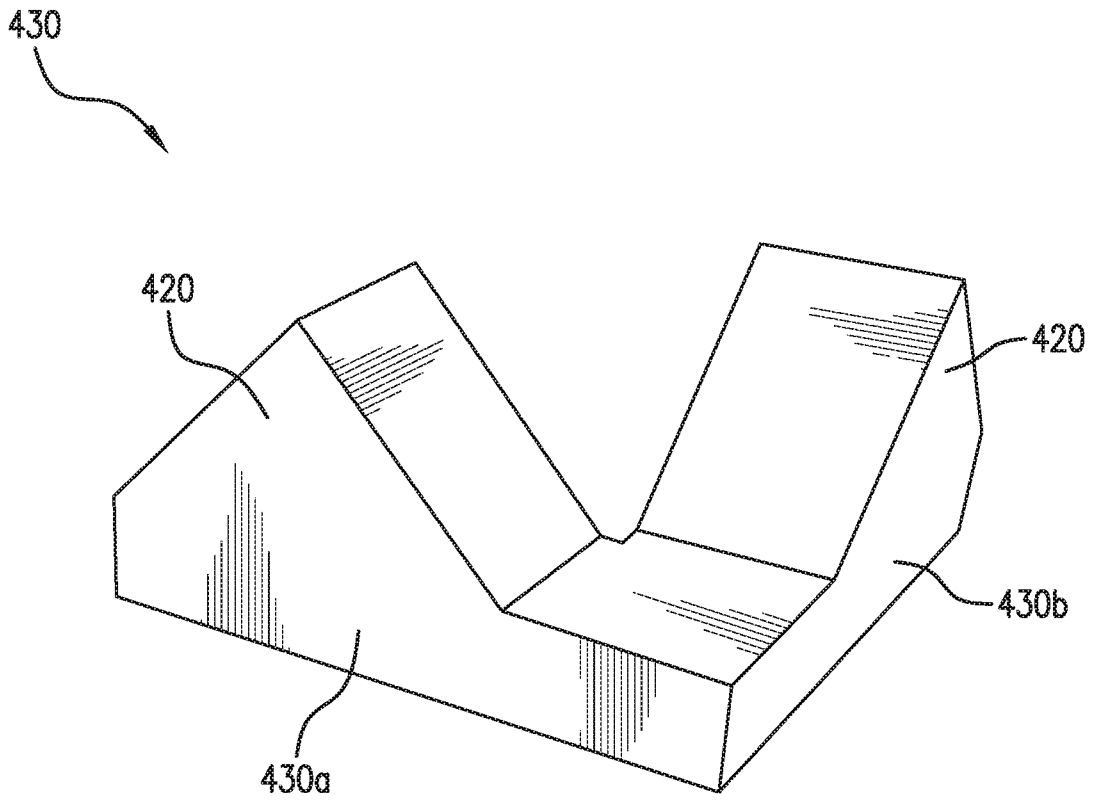


FIG. 7B

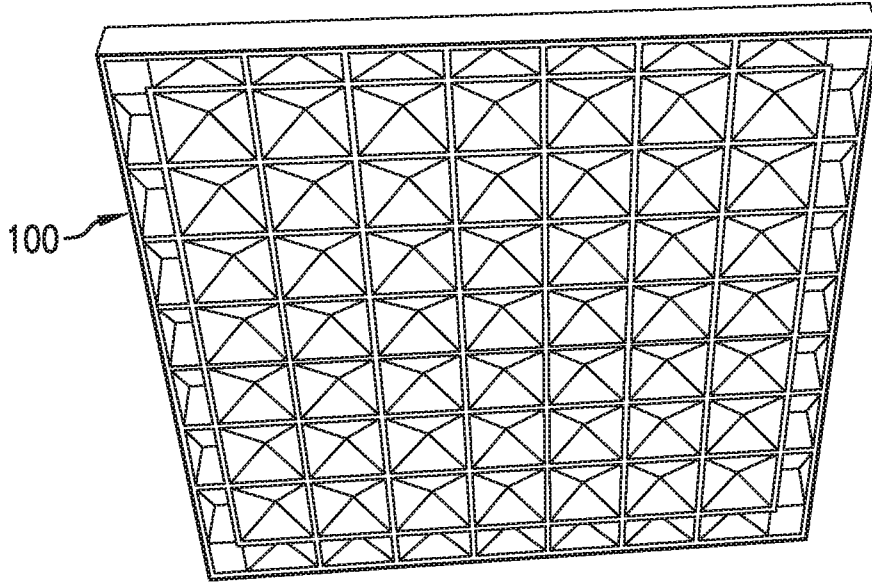


FIG. 8A

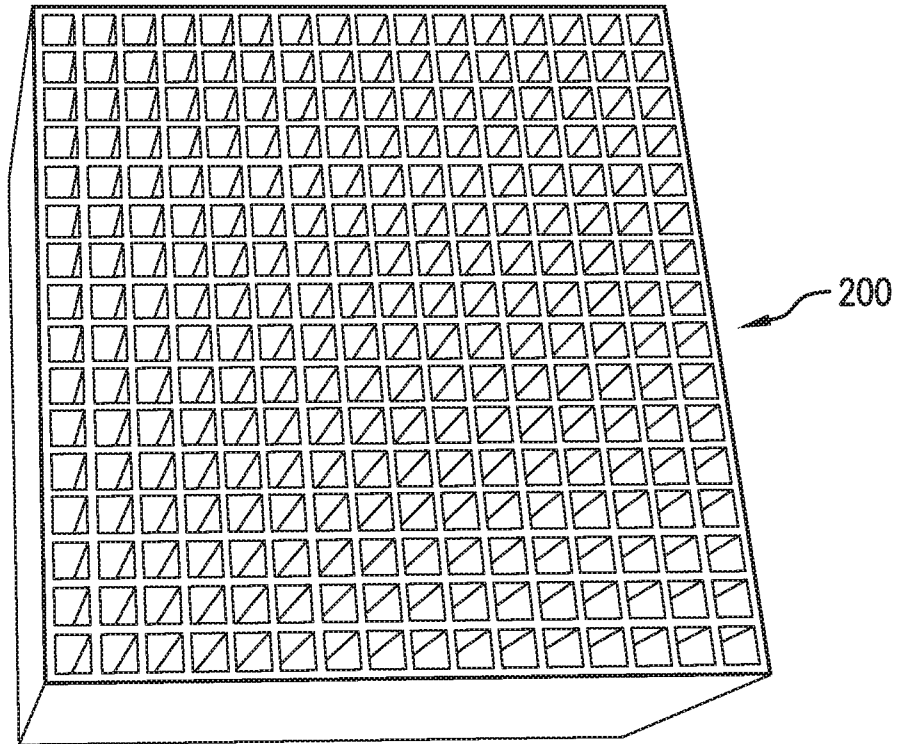


FIG. 8B

4-to-1 Uniform Glass

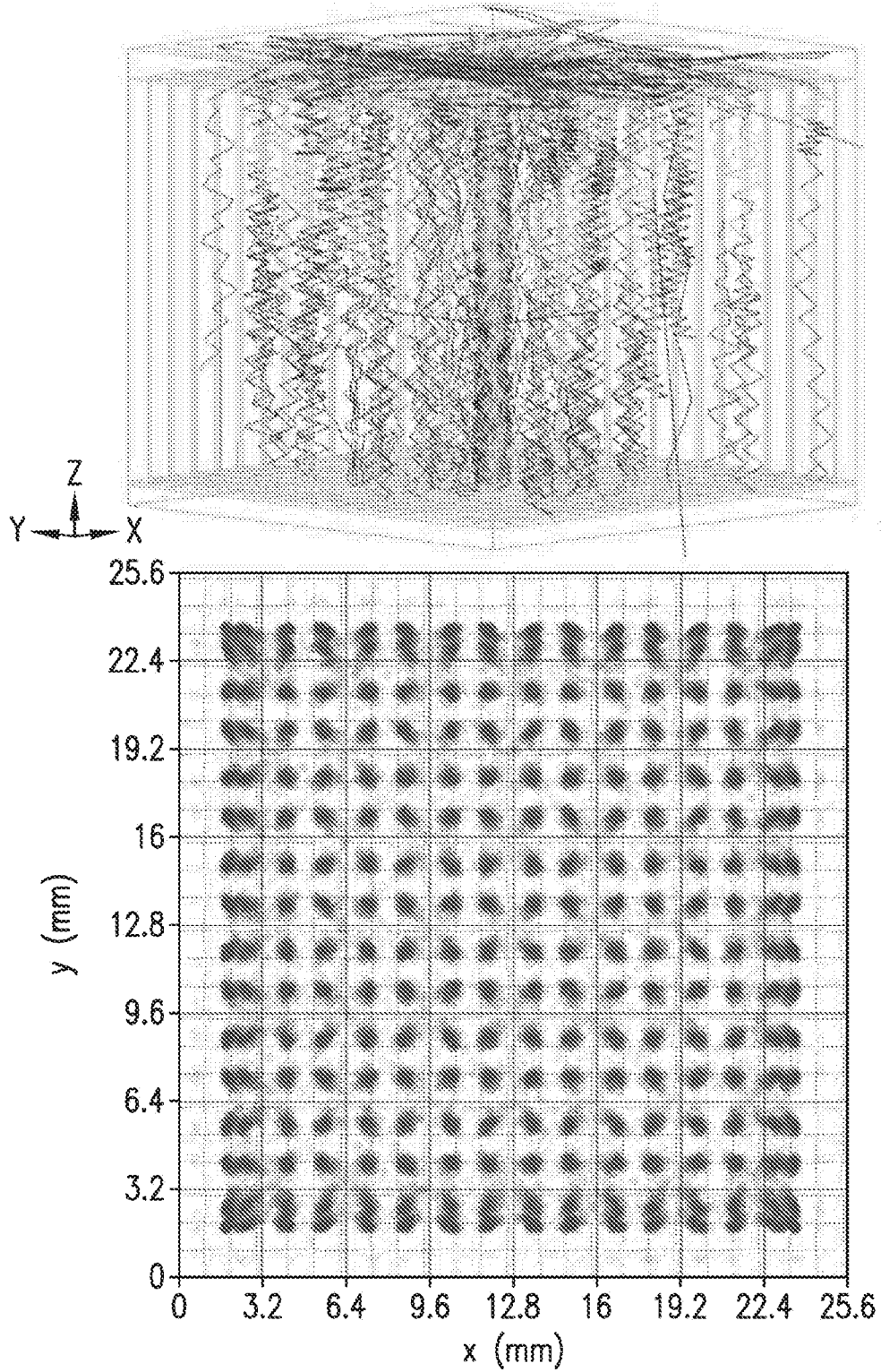


FIG.9A

4-to-1 Prism-PET

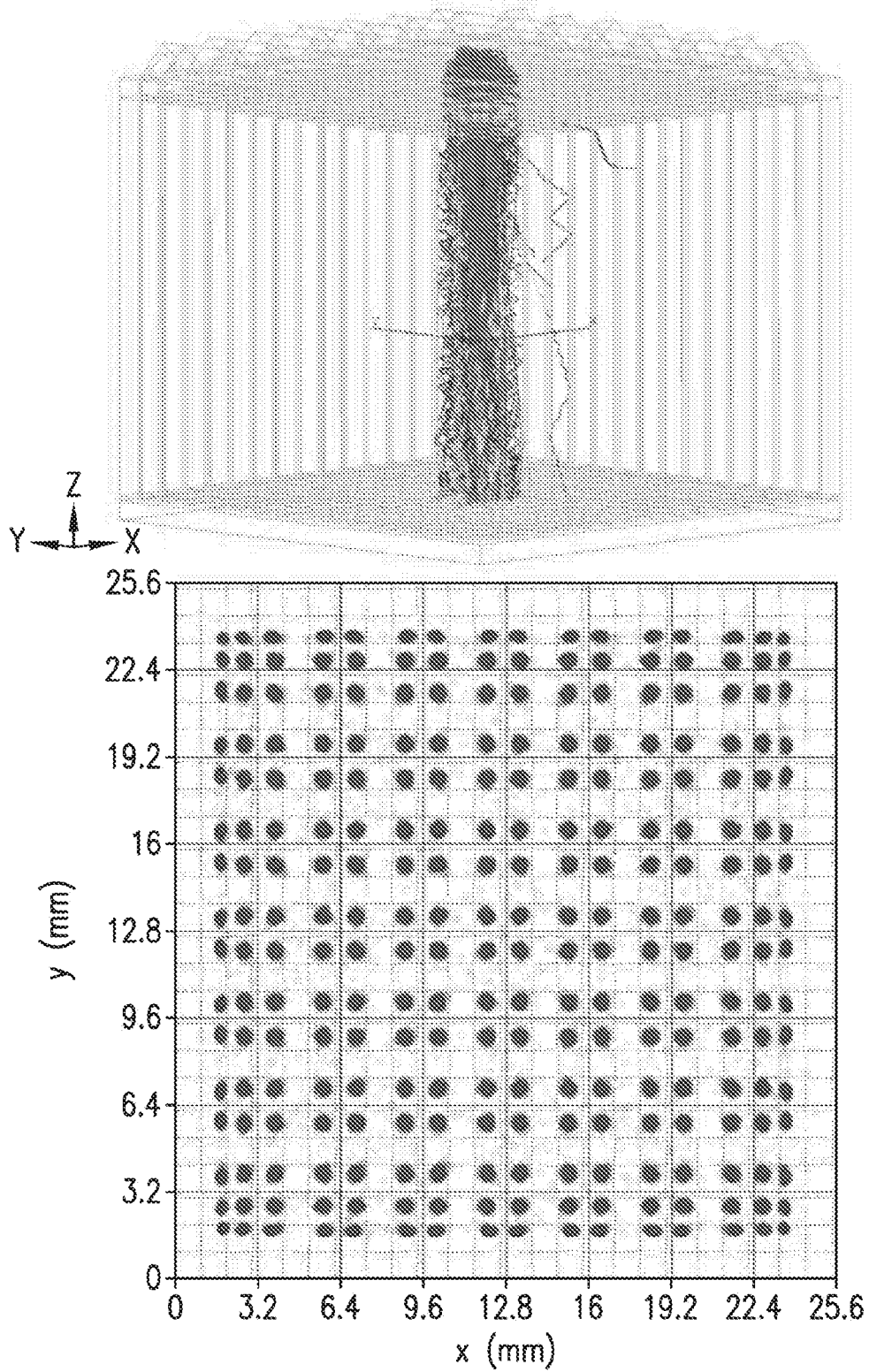


FIG.9B

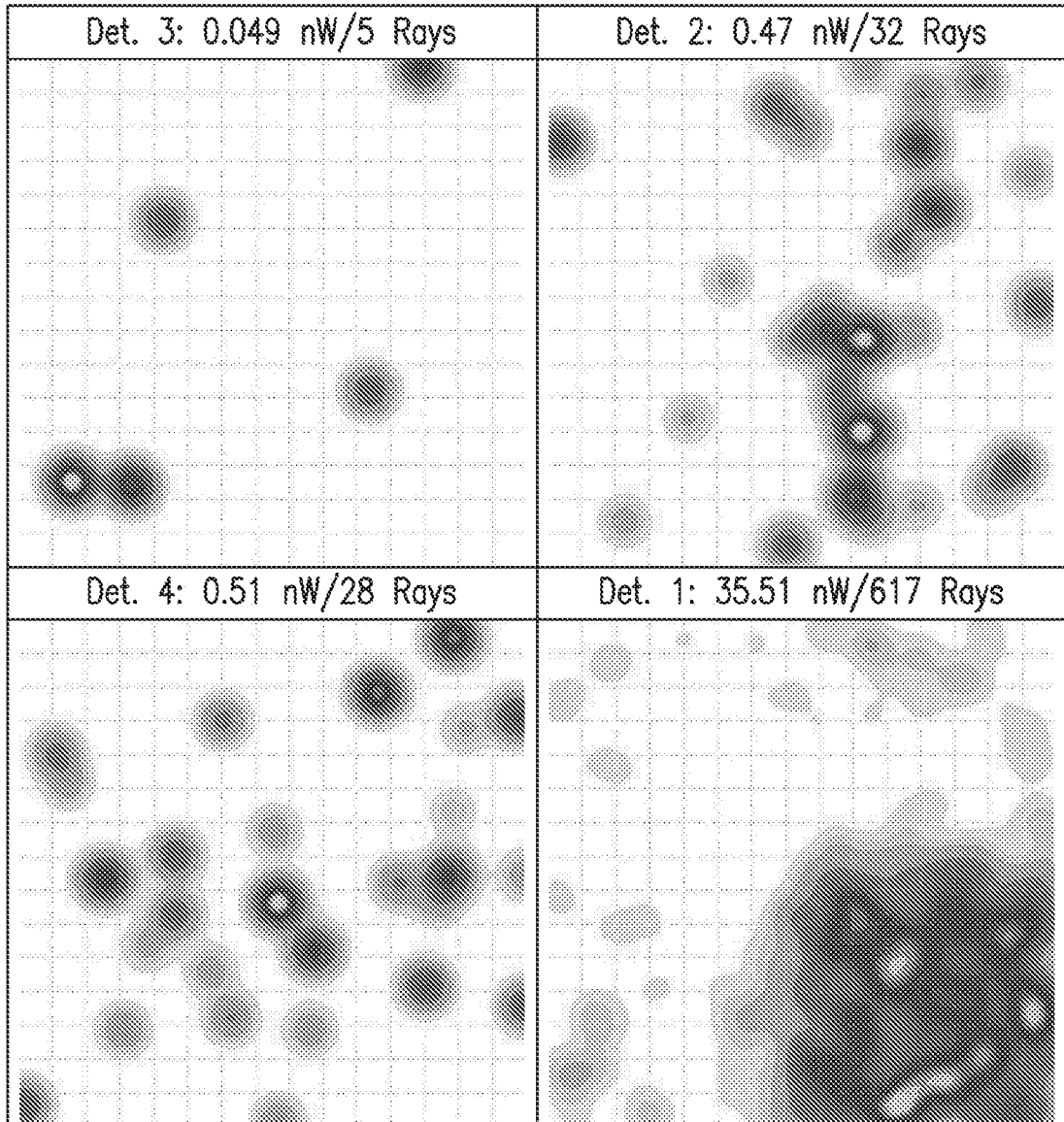


FIG. 10

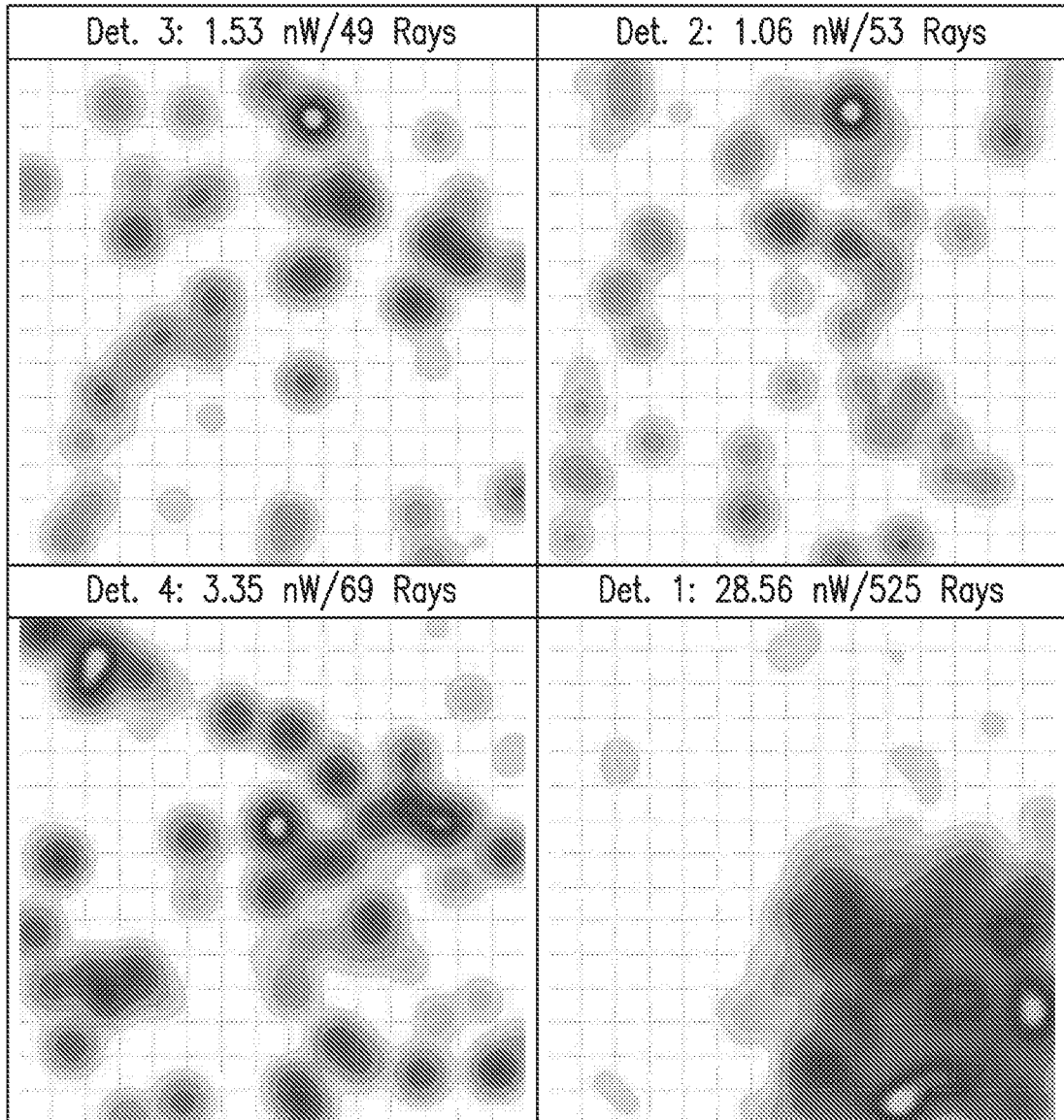


FIG. 11

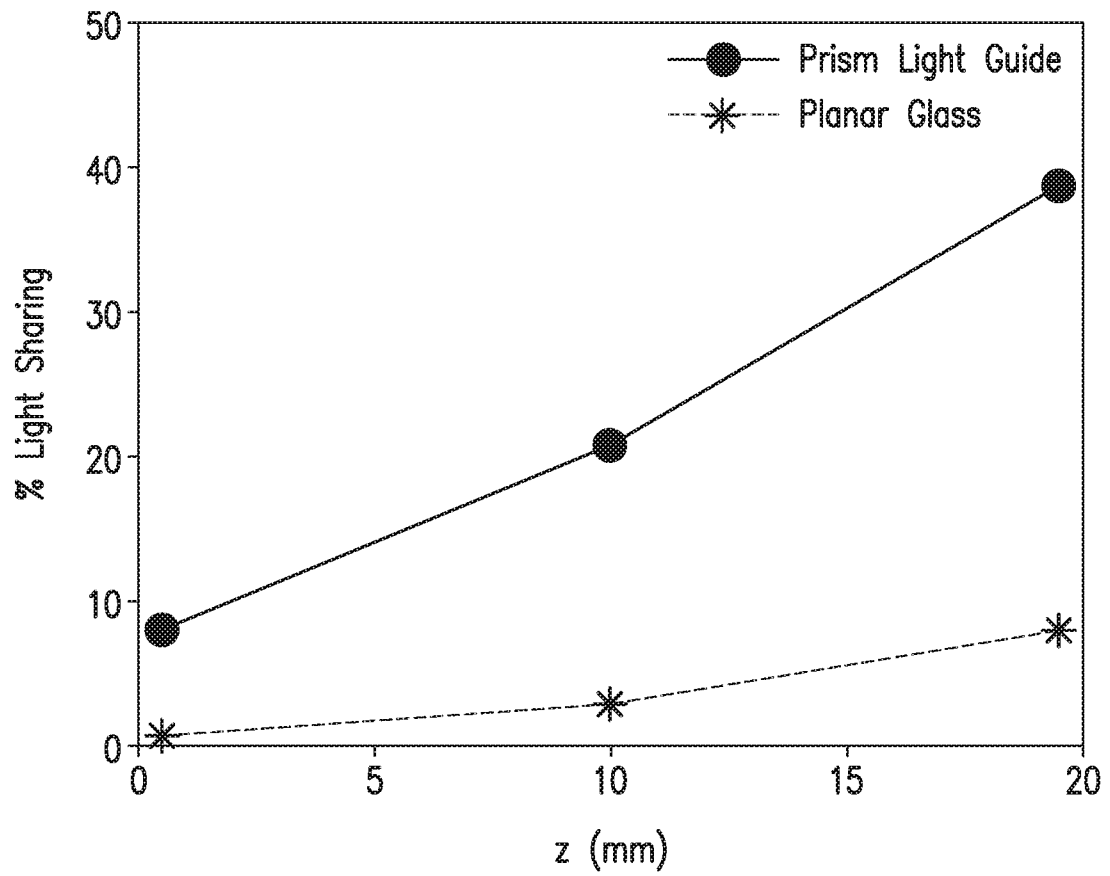


FIG. 12

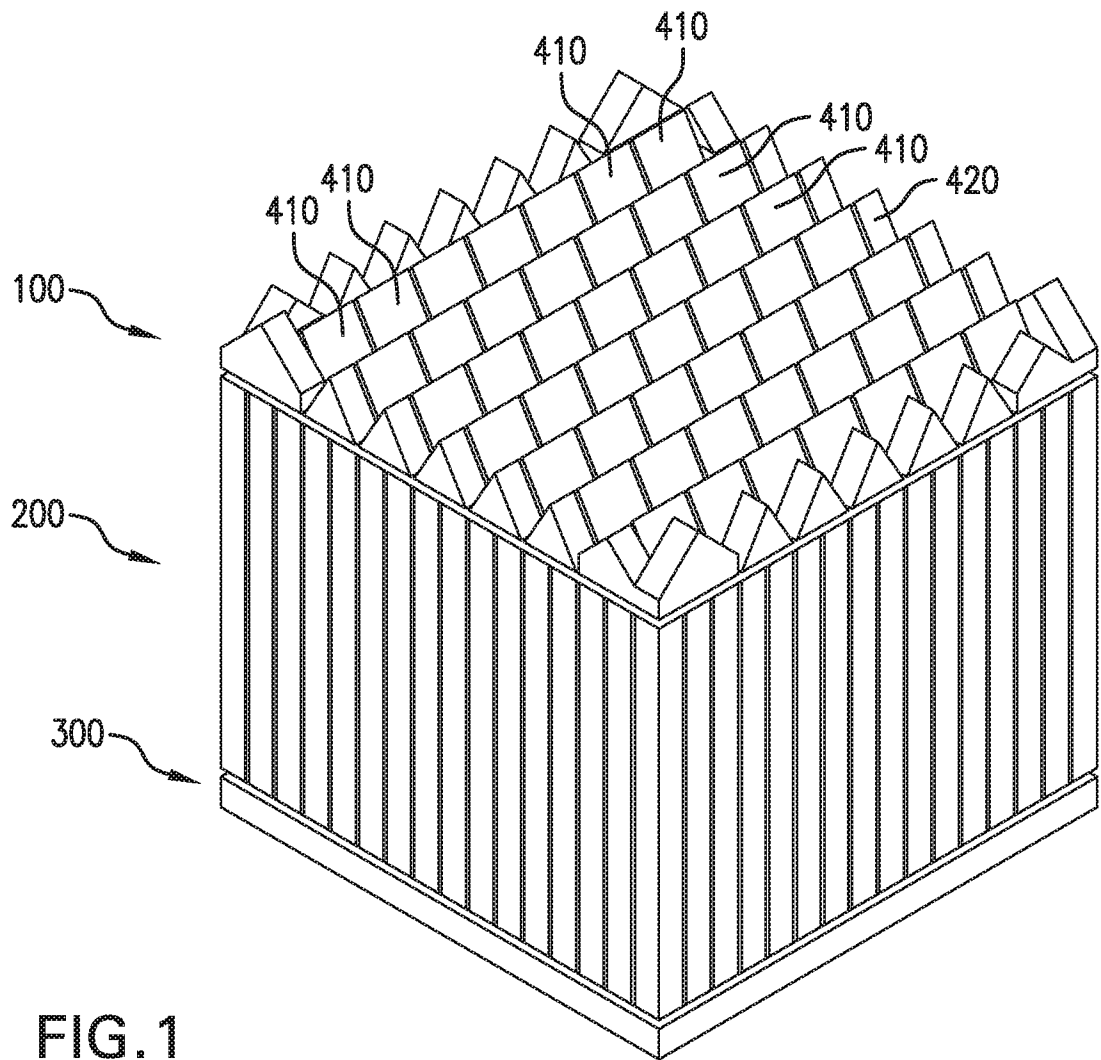


FIG. 1