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- (71) **Applicant:** KONINKLIJKE PHILIPS N.V. [NL/NL];  
High Tech Campus 5, NL-5656 AE Eindhoven (NL).
- (72) **Inventors:** HUANG, Kai; c/o High Tech Campus 5, NL-5656 AE Eindhoven (NL). WU, Ying; c/o High Tech Campus 5, NL-5656 AE Eindhoven (NL). DENG, Yinhuai; c/o High Tech Campus 5, NL-5656 AE Eindhoven (NL). LI, Xiaomin; c/o High Tech Campus 5, NL-5656 AE Eindhoven (NL).
- (74) **Agents:** STEFFEN, Thomas et al.; High Tech Campus 5, NL-5656 AE Eindhoven (NL).
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HN, HR, HU, ID, IL, IN, IS, JP, KE, KG, KN, KP, KR, KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA, ZM, ZW.

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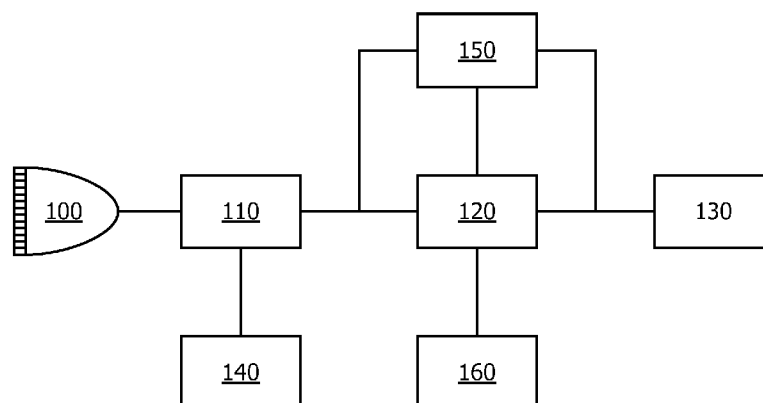
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- (54) **Title:** METHOD AND SYSTEM FOR PROCESSING ULTRASONIC IMAGING DATA

**FIG. 1**

(57) **Abstract:** The present invention provides a method and a system for processing ultrasonic data. The method comprises: obtaining (210) a B-mode ultrasonic image; setting (220) a first ROI on the ultrasonic image according to a first input received from a user; measuring (230) elasticity-related data for the first ROI by using a shear wave ultrasonic imaging technique; generating (240) a second ROI on the ultrasonic image on the basis of the first ROI; and extracting image features for the second ROI from the ultrasonic image.



## **METHOD AND SYSTEM FOR PROCESSING ULTRASONIC IMAGING DATA**

### **FIELD OF THE INVENTION**

5           The invention relates to an ultrasound-based imaging method and system, and particularly to the processing of ultrasonic imaging data.

### **BACKGROUND OF THE INVENTION**

10           Ultrasonic imaging has been widely accepted as an easy-to-use, inexpensive imaging modality to diagnose malignant cancers such as breast, liver, prostate cancers, etc. However, clinical doctors still have less confidence in the ability of using ultrasound to differentiate benign and malignant lesions because ultrasound has relatively poor image quality and operator-dependence compared to other imaging modalities such as computed tomography (CT) and Magnetic Resonance Imaging (MRI).

15           In recent years, a computer aided diagnosis (CAD) system, which is also referred to as computer decision support (CSD) system, has been developed to help clinical doctors to detect or diagnose lesions.

20           The current ultrasound-based CAD system relies on B-mode ultrasonic images. For example, anatomical information extracted from the B-mode ultrasonic images may be used for the computer aided diagnosis in a CAD system. In order to obtain the anatomical information of the relevant tissues, a user needs to manually set a region of interest (ROI) on the B-mode ultrasonic images. Then the anatomical information for the ROI may be extracted from the B-mode ultrasonic images and may be used for the computer aided diagnosis in the CDS system.

25           However, the anatomical information extracted from the B-mode ultrasonic images becomes insufficient for the CDS system. It is desirable to improve the performance of computer aided diagnosis by using for example another category of information in the ultrasound-based CAD system.

Ultrasonic elastography, for example a shear-wave ultrasonic imaging technique, is another ultrasonic imaging mode which can provide elasticity-related data (i.e., stiffness) of tissues. For example, Philips has developed the shear-wave ultrasonic elastography point quantification (elastoPQ) technique, which can provide quantitative mechanical information (i.e., stiffness) of tissues. In order to obtain the elasticity-related information of the relevant tissues, a user needs to manually set a ROI on the B-mode ultrasonic image to outline the relevant area, and then the shear-wave ultrasonic imaging procedure may be performed to obtain the elasticity-related information for the relevant area.

Our research results indicate that the combination of B-mode imaging technique and elastoPQ technique can improve the sensitivity and specificity of lesion detection and differentiation in the ultrasound-based CAD system. However, in order to obtain the anatomical information and the elasticity-related information, the user, such as the clinical doctor, needs to set the ROI for obtaining the anatomical information and the ROI for obtaining the elasticity-related information separately in the above-mentioned procedures to obtain the two kinds of information. In this way, the user's operation and experience are paramount to ensure that the two ROIs target the same relevant tissue area.

Therefore, it is desirable to provide a more efficient and reliable method and system for providing the two kinds of information to the ultrasound-based CAD system.

## SUMMARY OF THE INVENTION

For the sake of the above mentioned purpose, the present invention provides a method and system for facilitating the ultrasound-based computer aided diagnosis. The present invention can simplify the operation of the user for setting the two ROIs and make sure that the two ROIs target the same relevant tissue area.

According to an aspect of the present invention, a method of processing ultrasonic data is provided, the method comprising: obtaining a B-mode ultrasonic image; setting a first ROI on the ultrasonic image according to a first input received from a user; measuring elasticity

related data for the first ROI by using a shear wave ultrasonic imaging technique; generating a second ROI on the ultrasonic image on the basis of the first ROI; and extracting image features for the second ROI from the ultrasonic image.

In this method, through using the measurement box, i.e., the first ROI, for one mode of ultrasonic imaging, i.e., shear wave ultrasonic imaging (elastoPQ as an example) as the basis for generating the second ROI for the processing of another mode of ultrasonic images, i.e., B-mode ultrasonic images, the user only needs to set the ROI once and the second ROI is automatically generated based on the ROI set by the user. In this way, the user operation is simplified and the first and second ROIs are sure to target the same or a corresponding relevant tissue area with respect to the two kinds of information, i.e., the elasticity-related information and the anatomical information.

According to an embodiment of the present invention, the method further comprises receiving a second input from the user.

In this embodiment, the step of generating the second ROI comprises:

if the second input indicates a lesion application, generating, on the basis of the first ROI, a contour of the lesion in the ultrasonic image as the second ROI;

if the second input indicates a non-lesion application, generating the second region of interest around the first ROI as the second ROI according to a predetermined shape.

In this embodiment, through generating the second ROI in different ways according to the related clinical applications, the second ROI may be set in a more accurate manner.

According to an embodiment of the present invention, the step of generating a predetermined shape around the first ROI as the second ROI comprises: using the first ROI as the second ROI; or generating the second region of interest by expanding from the first ROI by a predetermined factor.

In this embodiment, for the non-lesion application, the simplest way to generate the second ROI is to use the first ROI as the second ROI. In this way the processing complexity may be reduced.

According to an embodiment of the present invention, the method further comprises

receiving a third input from the user, and adjusting the second ROI according to the third input received from the user.

In this embodiment, the user is allowed to adjust the generated second ROI manually.

According to another aspect of the present invention, a system for processing ultrasonic data is provided, the system comprising: an ultrasonic probe; a B-mode imaging unit for obtaining a B-mode ultrasonic image from ultrasonic radio-frequency data collected by the ultrasonic probe; a user interface for receiving a first input of a user and setting a first ROI on the ultrasonic image according to the first user input; an elasticity measuring unit for measuring elasticity-related data for the first ROI by using a shear wave ultrasonic imaging technique; and an image processing unit for generating a second ROI on the ultrasonic image on the basis of the first ROI and extracting image features for the second ROI from the ultrasonic image.

In this aspect, the present invention provides a system in which the elasticity-related information and the anatomical information may be efficiently obtained and reliably relate to the same or a corresponding relevant tissue area . And in this system, the user only needs to set the first ROI once and the second ROI is automatically generated by an image processing unit, based on the first ROI; in this way the user operation is simplified and two ROIs are sure to target the same or a corresponding relevant tissue area.

According to an embodiment of the present invention, the user interface is adapted for receiving a second user input.

And in this embodiment, the image processing unit may be adapted for:

if the second input indicates a lesion application, generating, on the basis of the first ROI, a contour of the lesion in the ultrasonic image as the second ROI;

if the second input indicates a non-lesion application, generating the second region of interest around the first ROI according to a predetermined shape.

And in this embodiment, the image processing unit may be further adapted for: using the first ROI as the second ROI, or for generating the second region of interest by expanding from the first ROI by a predetermined factor.

According to an embodiment of the present invention, the user interface may be adapted for receiving a third input from the user and adjusting the second ROI according to the third input received from the user.

According to another aspect of the present invention, a computer program product is provided comprising machine executable instruction codes which, when executed on a machine, cause the machine to perform the above mentioned methods for processing ultrasonic data.

According to another aspect of the present invention, an ultrasonic imaging apparatus is provided which comprises an image processor for processing ultrasonic data, the image processor being configured to perform the above mentioned methods.

Other objects and advantages of the present invention will become more apparent from and will be easily understood with reference to the description made in combination with the accompanying drawings.

## DESCRIPTION OF THE DRAWINGS

The present invention will be described and explained hereinafter in more detail by means of embodiments and with reference to the drawings, in which:

Fig. 1 is a block diagram which illustrates an ultrasonic diagnostic imaging system constructed in accordance with an embodiment of the present invention;

Fig. 2 is a flowchart of a method for the combined use of shear-wave ultrasonic imaging technique and B-mode ultrasonic imaging technique in accordance with an embodiment of the present invention.

The same reference signs in the figures indicate similar or corresponding features and/or functionalities.

## DETAILED DESCRIPTION

Embodiments of the present invention will be described hereinafter in more detail with reference to the drawings.

Referring to Fig. 1, an ultrasonic system constructed in accordance with an embodiment of the present invention is shown in the block diagram.

An ultrasonic probe 100 has a transducer array of transducer elements for transmitting and receiving ultrasonic signals. The transducer array can be a one-dimensional or a two-dimensional array of transducer elements. Either type of transducer array can scan a two-dimensional (2D) plane and the two-dimensional array can be used to scan a volumetric region in front of the array.

The ultrasonic probe 100 is coupled to a B-mode imaging unit 110. The B-mode imaging unit 110 may obtain B-mode ultrasonic images from the ultrasonic radio-frequency data collected by the ultrasonic probe 100. The obtained B-mode ultrasonic images may be displayed on the display 150 which is coupled to the B-mode imaging unit 110. And the obtained B-mode ultrasonic images may also be further processed in the image processing unit 120 which is coupled to the B-mode imaging unit 110.

While viewing the displayed B-mode ultrasonic image, a user such as a clinical doctor or a radiologist may set a first ROI on the B-mode ultrasonic image via the user interface 130, which is coupled to the image processing unit 120 and/or to the elasticity measuring unit 140 (not shown in the fig.1). In other words, the user interface may receive a user input and set a first ROI on the ultrasonic image according to the user input. The first ROI set via the user interface may be used by the elasticity measuring unit 140 to perform the measurement of elasticity-related data for the first ROI. The measurement of elasticity-related data may be performed by using a shear wave ultrasonic imaging technique. Such a shear wave ultrasonic imaging technique is described in Philips's patent application WO2011/064688, which is referred to in this application. And the measurement of elasticity-related data may be performed by using the shear-wave ultrasonic elastography point quantification (elastoPQ) technique developed by Phillips. Then the measured elasticity-related data may be provided to the CDS system 160 for the purpose of computer aided diagnosis.

The image processing unit 120 may generate a second ROI on the ultrasonic image on

the basis of the first ROI set via the user interface. And the image processing unit 120 may perform further processing of the B-mode ultrasonic images with respect to the second ROI. According to an embodiment, the image processing unit 120 may extract image features for the second ROI from the B-mode ultrasonic images. The extracted image features may present the anatomical information of the relevant tissue area outlined by the second ROI; for example, the image features extracted for the second ROI may be morphological features, texture features, margin features and so on, which may be provided in the CDS system 160 for the purpose of computer aided diagnosis.

In the above embodiment, the extraction of image features is performed by the image processing unit 120 outside the CDS system 160. However, in a variation of the embodiment, the functional unit for extracting image features may be implemented in the CDS system 160. In this variation of embodiment, the image processing unit 120 may provide the B-mode ultrasonic images having the second ROI thereon to the CDS system 160, and a feature extracting unit of the CDS system may extract the image features for the second ROI from the B-mode ultrasonic images.

In the above embodiment, the measured elasticity-related data and the extracted image features are provided to the CDS system 160 for the computer aided diagnosis. However, it should be understood that the CDS system should not be considered as a necessary component for the implementation of the system of the present invention. For example, the measured elasticity-related data and the extracted image features may be displayed to the user just for facilitating the user's diagnosis. And in another example, the measured elasticity-related data and the extracted image features may be simultaneously displayed to the user and provided to the CDS system.

In an embodiment, the image processing unit 120 may generate the second ROI in different manners according to different clinical applications. In this embodiment, the user may specify, via the user interface 130, what kind of clinical application the present diagnosis relates to; in other words, the user interface may present a prompt to the user to select the type of clinical application and receive a user input, which is referred to as a second user input



hereafter.

If the second input indicates that the application is a lesion application, for example, to differentiate malignant lesion from cirrhosis nodule, then the image processing unit 120 may generate a contour of the lesion in the ultrasonic image on the basis of the first ROI for measuring elasticity information and use the contour as the second ROI for extracting anatomical information. In order to accurately measure the elasticity information of the relevant tissue area, such as a lesion, the user typically needs to set the first ROI within the lesion area. Therefore, the contour of the lesion area may be generated by a segmentation technique based on the first ROI. For example, the segmentation technique may use the first ROI as the initial contour and achieve the contour of the lesion by expanding the initial contour to the real contour. It should be understood that in order to achieve the contour of the lesion, it is not compulsory to set the first ROI perfectly within the lesion area. The contour of the lesion may be achieved as long as the first ROI roughly overlaps the lesion area. An exemplary segmentation technique for detecting a contour of a subject on the basis of an initially set contour which roughly covers the subject is provided in “Localizing Region-Based Active Contours”, Shawn Lankton, et al, IEEE TRANSACTIONS ON IMAGE PROCESSING, VOL.17, NO.11, NOVEMBER 2008, which is referred to in this application. And the exemplary segmentation technique may be used by the image processing unit to generate the contour of the lesion on the basis of the first ROI. In an example, after the contour is generated as the second ROI, it may be desirable for the user to manually adjust the second ROI, and in some cases manual adjustment by the user might be needed. Therefore, in this example, the user may be allowed to adjust the second ROI via the user interface; in other words, the user interface may receive further input from the user and adjust the second ROI according to the user’s input.

If the second input indicates that the application is a non-lesion application, for example, to classify liver cirrhosis, distinguish fatty liver from normal liver, then the image processing unit 120 may generate the second ROI in a different way. For example, the image processing unit 120 may generate the second ROI around the first ROI according to a predetermined

shape. In an example, the image processing unit may use the first ROI as the second ROI. In another example, the image processing unit may expand the first ROI by a predetermined factor and use the expanded shape from the first ROI as the second ROI. The factor may be an experimental value and may be set beforehand. In an example, the user is allowed to adjust  
5 the factor via the user interface in order to adjust the expanded shape; in other words, the user interface may receive further user input and adjust the second ROI according to the user input.

It is described in the above embodiment that different ways are used to generate the second ROI according to different clinical applications. However, the present invention is not limited to a specific way of generating the second ROI. For example, any way of generating  
10 the second ROI as described above may be used in any clinical application. And other ways to generate the second ROI based on the first ROI are also applicable in the present invention.

Referring to Fig. 2, a method for combined use of a shear-wave ultrasonic imaging technique and a B-mode ultrasonic imaging technique is shown in the block diagram.

15 At step 210, a B-mode ultrasonic image may be obtained.

At step 220, a first ROI may be set on the ultrasonic image according to a first input received from a user.

At step 230, elasticity-related data for the first ROI may be measured by using a shear wave ultrasonic imaging technique.

20 At step 240, a second ROI may be generated on the ultrasonic image on the basis of the first ROI.

At step 250, image features may be extracted for the second ROI from the ultrasonic image.

Although the steps of the method are shown as sequential steps, it should be understood  
25 that the present invention is not limited to the specific sequence of the steps. For example, step 230 may be performed in parallel with steps 240 and 250.

According to an embodiment of the present invention, the second ROI may be generated in different ways according to different clinical applications. In this embodiment, before

generating the second ROI at step 240, the method may further comprise receiving a second input from the user. If the second input indicates a lesion application, then at step 240, a contour of the lesion in the ultrasonic image may be generated on the basis of the first ROI and may be used as the second ROI. If the second input indicates a non-lesion application, the second ROI may be generated in a different way at step 240; for example, the second ROI around the first ROI may be generated according to a predetermined shape. In an example, the first ROI may be used as the second ROI. In another example, the first ROI may be expanded by a predetermined factor and the shape expanded from the first ROI may be used as the second ROI. The factor may be an experimental value and may be set beforehand. And, in an example, a third input may be received from the user, and the second ROI may be adjusted according to the third input received from the user.

It should be understood that some units as shown in fig.1 may be implemented in a processor, or may be implemented in several hardware components; for example, the B-mode ultrasonic imaging unit 110, the image processing unit 120 and the shear wave ultrasonic imaging unit 140 may be implemented respectively in a dedicated processing unit such as a Digital Signal Processor (DSP) or an Application Specific Integrated Circuit (ASIC) or the like designed specifically for implementing their functions.

It should be understood that method 200 as shown in fig.2 may be implemented in software as a computer program product, the described process may be stored on or transmitted as program instructions or codes on a computer-readable medium. And a processor such as a general purpose processor or a specific purpose processor may be used, when executing the program instructions, to perform the method as described above. Computer-readable media include any medium that facilitates transfer of a computer program from one place to another and that can be accessed by a computer. By way of example, the computer-readable media may include RAM, ROM, EEPROM, CD-ROM or other optical disk storage, magnetic disk storage or other magnetic storage devices, or any other medium that can be used to carry or store desired program codes in the form of instructions or data

structures and that can be accessed by a computer.

It should be noted that the above-mentioned embodiments illustrate rather than limit the invention and that those skilled in the art will be able to design alternative embodiments without departing from the scope of the appended claims. In the claims, any reference signs  
5 placed between parentheses shall not be construed as limiting the claim. The word “comprising” does not exclude the presence of elements or steps not listed in a claim or in the description. The word “a” or “an” preceding an element does not exclude the presence of a plurality of such elements. In the system claims enumerating several units, several of these units can be embodied by one and the same item of software and/or hardware. The usage of  
10 the words first, second and third, et cetera, does not indicate any ordering. These words are to be interpreted as names.

## CLAIMS:

1. A method of processing ultrasonic data, comprising:
  - Obtaining (210) a B-mode ultrasonic image;
  - Setting (220) a first region of interest on the ultrasonic image according to a first input received from a user;
  - Measuring (230) elasticity-related data for the first region of interest by using a shear wave ultrasonic imaging technique;
  - Generating (240) a second region of interest on the ultrasonic image on the basis of the first region of interest; and
  - Extracting (250) image features for the second region of interest from the ultrasonic image.
2. The method according to claim 1, further comprising receiving a second input from the user,
  - wherein generating the second region of interest comprises:
    - if the second input indicates a lesion application, generating, on the basis of the first region of interest, a contour of the lesion in the ultrasonic image as the second region of interest;
    - if the second input indicates a non-lesion application, generating the second region of interest around the first region of interest according to a predetermined shape.
3. The method according to claim 2, wherein generating the second region of interest around the first region of interest according to the predetermined shape comprises:
  - using the first region of interest as the second region of interest; or
  - generating the second region of interest by expanding from the first region of interest by a predetermined factor.

4. The method according to claim 2, further comprising:  
receiving a third input from the user; and  
adjusting the second region of interest according to the third input received from the user.

5. A system for processing ultrasonic data, comprising:  
an ultrasonic probe (100);  
a B-mode imaging unit (110) for obtaining a B-mode ultrasonic image from ultrasonic radio-frequency data collected by the ultrasonic probe;  
a user interface (130) for receiving a first input of a user and setting a first region of interest on the ultrasonic image according to the first user input;  
an elasticity measuring unit (140) for measuring elasticity-related data for the first region of interest by using a shear wave ultrasonic imaging technique; and  
an image processing unit (120) for generating a second region of interest on the ultrasonic image on the basis of the first region of interest, and extracting image features for the second region of interest from the ultrasonic image.

6. The system according to claim 5, wherein the user interface (130) is adapted for receiving a second user input,

wherein the image processing unit (120) is adapted for:

if the second input indicates a lesion application, generating, on the basis of the first region of interest, a contour of the lesion in the ultrasonic image as the second region of interest;

if the second input indicates a non-lesion application, generating the second region of interest around the first region of interest according to a predetermined shape.

7. The system according to claim 6, wherein the image processing unit (120) is further adapted for:

using the first region of interest as the second region of interest; or

generating the second region of interest by expanding from the first region of interest by a predetermined factor.

8. The system according to claim 6, wherein the user interface (130) is adapted for receiving a third input from the user and adjusting the second region of interest according to the third input received from the user.

9. A computer program product comprising instruction codes for performing the method according to any one of claims 1 to 4.

10. An ultrasonic imaging apparatus comprising  
an image processor for processing ultrasonic data, the image processor being configured to perform the method according to any one of claims 1 to 4.

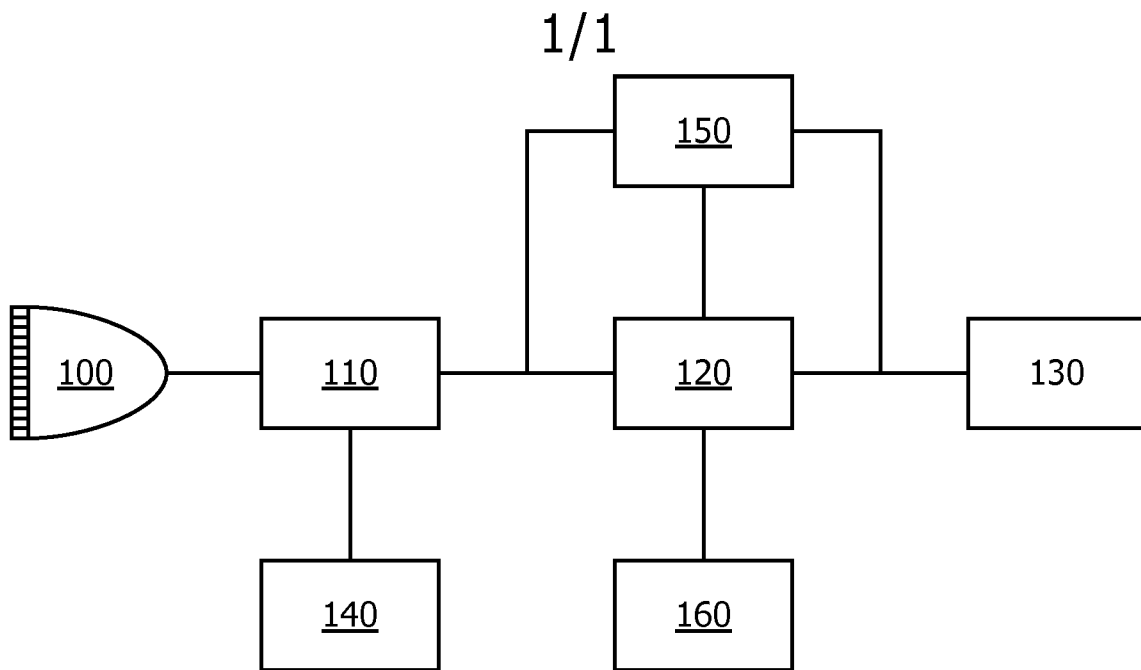


FIG. 1

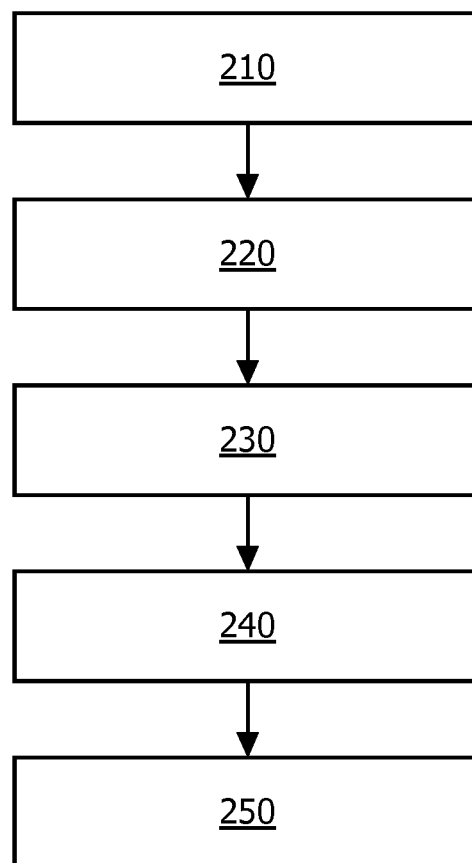


FIG. 2



# INTERNATIONAL SEARCH REPORT

International application No  
PCT/IB2013/055382

A. CLASSIFICATION OF SUBJECT MATTER  
INV. A61B8/00  
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)  
A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EP0-Internal, WPI Data

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

| Category* | Citation of document, with indication, where appropriate, of the relevant passages  | Relevant to claim No. |
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| X         | -----<br>US 2010/317971 A1 (FAN LIEXIANG [US] ET AL) 16 December 2010 (2010-12-16) paragraphs [0010], [0025] - [0026], [0035] - [0037], [0039], [0048], [0049], [0055], [0056], [0057], [0095]; figures 1,3,4 | 1,5,9,10              |
| X         | -----<br>US 2011/306884 A1 (TANIGAWA SHUNICHIRO [JP] ET AL) 15 December 2011 (2011-12-15) paragraphs [0062], [0063], [0068], [0069], [0073]; figures 1-4  | 1,5,9,10              |
|           | -----<br>-/--   |                       |

☒ Further documents are listed in the continuation of Box C.

☒ See patent family annex.

\* Special categories of cited documents:

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"E" earlier application or patent but published on or after the international filing date

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"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search

31 October 2013

Date of mailing of the international search report

13/11/2013

Name and mailing address of the ISA/

European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040,  
Fax: (+31-70) 340-3016

Authorized officer

Daoukou, Eleni

# INTERNATIONAL SEARCH REPORT

International application No  
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C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

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| A         | US 2011/152687 A1 (IIMURA TAKASHI [JP] ET AL) 23 June 2011 (2011-06-23) paragraphs [0012], [0056], [0063], [0064], [0067]; figures 2,4<br>-----         | 3,7                   |

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

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| Patent document<br>cited in search report | Publication<br>date | Patent family<br>member(s) | Publication<br>date |
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