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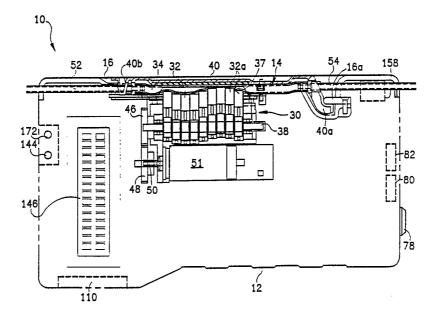
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(54) Title: DISPOSABLE INFUSION APPARATUS WITH PERISTALTIC PUMP



(57) Abstract

A disposable infusion apparatus (10) includes proximal, distal and intermediate segments of IV tubing (14) connected via couplings (20, 26). The intermediate segment (34) has a length sufficient for operative engagement with a pumping member (32) of a peristaltic pump throughout a pumping stroke thereof. The intermediate segment (34) further has a maximum Durometer of seventy-five on the Shore A scale. The pumping member (32) includes a plurality of fingers (32a) mounted in side-by-side substantially parallel relationship for individual reciprocation. Motor driven cams (36) individually reciprocate respective ones of the fingers in a predetermined timed sequence so that when the linearly disposed intermediate segment (34) is squeezed by the fingers (32a), intravenous fluid in the tubing will be pumped therethrough. The disposable apparatus (10) further includes a door (40) connected to opposite ends of the intermediate segment (34) and which is releasably loadable in a case (12) to place the intermediate segment into operative engagement with the pumping member.

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Description

Disposable Infusion Apparatus With Peristaltic Pump

Reference To Related Applications

This application is related to co-pending U.S. Patent Application Serial No. 07/518,987, entitled "PROGRAMMABLE INFUSION SYSTEM", filed on May 4, 1990.

5

Technical Field

The present invention relates to medical devices, and more particularly, to an improved disposable infusion apparatus and peristaltic pump for delivering 10 intravenous drugs at a controlled rate to a patient.

Background Art

It is often necessary to intravenously supply patients with pharmaceutically active liquids over a long period of time at a controlled rate. It is desirable that this be accomplished while the patient is in an ambulatory state.

The prior art includes devices that employ a bag filled with fluid medication that feeds by gravity 20 through IV tubing having drip or other controllers. It is difficult for a patient to be ambulatory with a gravity fed infusion device and flow control is very limited.

Another prior art infusion apparatus comprises an 25 elastic bladder forming a liquid container mounted in an elongated cylindrical housing, a flow control valve, and tubing for supply of the liquid to the patient. The elastic walls of the bladder expand along the walls of the cylindrical housing when filled 30 with the liquid, and provide the pressure for

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expelling the liquid. The bladder is typically filled by hand with a syringe which often requires an inordinate amount of force. Another drawback is that the bladder is forced to expand into an unnatural 5 elongated configuration along the housing walls as it filled. As result of this unnatural a configuration, the pressure of the bladder varies widely with the volume of liquid therein. Therefore, in most cases this type of elastic infusion apparatus 10 does not have a reasonably stable pressure and flow rate over the infusion period.

Most of such devices either have a flow rate that decreases with pressure, which decreases with volume, or one that remains roughly constant until the end where it surges. Attempts have been made to control pressure and flow rates by means of complicated and expensive flow control valves and devices. Other approaches have utilized exotic and expensive elastic materials in an effort to control the pressures and flow rates.

Another type of infusion apparatus employs a peristaltic or other positive displacement pump which is electrically driven. Programmable infusion pumps have been provided having the capability for precise 25 tailoring of the fluid delivery rate parameters in different modes, namely, continuous, intermittent, PCA (patient controlled analgesic) and (total parenteral nutrition). Originally such programmable infusion pumps were large and not well 30 suited for ambulatory patients. They used complex and expensive replacement pump cartridges to maintain sterility. More recently, small programmable infusion pumps have been available with disposable plastic cartridges that engage a peristaltic pump. However

such cartridges have been bulky and expensive and have required excessive drive power in the pumps, leading to rapid battery drain.

Accordingly, it would be desirable to provide an 5 improved disposable infusion apparatus and pump for delivering intravenous drugs at a controlled rate to an ambulatory patient.

Disclosure of Invention

It is therefore the primary object of the present invention to provide an improved disposable infusion apparatus and pump for delivering intravenous drugs at a controlled rate to an ambulatory patient.

In accordance with our invention a disposable 15 infusion apparatus includes proximal, distal intermediate segments of IV tubing connected via The intermediate segment has a length couplings. sufficient for operative engagement with a pumping member of a peristaltic pump throughout a pumping 20 stroke thereof. The intermediate segment further has a maximum Durometer of seventy-five on the Shore A scale. The pumping member includes a plurality of fingers mounted in side-by-side substantially parallel reciprocation. individual for relationship 25 driven cams individually reciprocate respective ones of the fingers in a predetermined timed sequence so that when the linearly disposed intermediate segment is squeezed by the fingers, intravenous fluid in the tubing will be pumped therethrough. The disposable door connected to includes a 30 apparatus further opposite ends of the intermediate segment and which is case to place the releasably loadable in a intermediate segment into operative engagement with the pumping member.

Brief Description of Drawings

The above and other objects and advantages of the present invention will become apparent from the following description when read in conjunction with 5 the accompanying drawings wherein:

Fig. 1 illustrates a programmable infusion system in phantom lines with a preferred embodiment of our disposable apparatus loaded therein. The disposable is shown connected to conventional IV tubing segments, an IV bag, a spike connector and a leur fitting. The IV tubing segments are broken at various locations to make this figure more compact.

Fig. 2 is an enlarged fragmentary view of the programmable infusion system with the disposable showing installed therein 15 apparatus and its relationship to a preferred embodiment of our peristaltic pump.

Fig. 3 is a further enlarged view of the peristaltic pump and the door of the disposable. The 20 IV tubing segments are not shown in this figure.

Fig. 4 is an enlarged view of the three segments of tubing that form part of the disposable.

Fig. 5 is an enlarged side elevation view of one of the fingers of the peristaltic pump showing how it 25 squeezes shut the intermediate tubing segment of the disposable.

Fig. 6 is a side elevation view of one of the cam wheels of the peristaltic pump. The motion of the cam wheel is illustrated in phantom lines.

Figs. 7-9 illustrate details of the disposable door, tube clamp and IV tubing couplings.

Best Mode for Carrying Out the Invention

Referring to Fig. 1, a programmable infusion system 10 is illustrated which is adapted to utilize our disposable infusion apparatus and peristaltic pump. It includes a compact, portable rectangular case 12. By way of example, the case may be made of injection molded plastic and may measure approximately seven inches in length by approximately three and one-half inches in width (right side in Fig. 1) by approximately one inch in thickness (right side in Fig. 1).

The preferred embodiment of our disposable IV tubing apparatus 14 (Fig. 2) may be releasably loaded or installed in a receptacle 16 (Fig. 2) in a long 15 side edge of the case 12. The proximal end disposable IV tubing apparatus 14 is connected to a conventional spike 20 (Fig. 1). The patient inserts the spike into a conventional bag 22 of intravenous fluid in which the desired medications are dissolved. The distal end 20 of the disposable IV tubing apparatus 14 is connected to a conventional male leur fitting 26 which in turn conventional IV catheter connects to a A disposable IV fluid conveying means illustrated). is a necessary requirement in an infusion system since 25 it ensures sterility. It also prevents residual amounts of medication from one IV drug administration from being inadvertently delivered when a new IV drug administration commences.

Referring to Fig. 2, the preferred embodiment of 30 our peristaltic pump 30 is mounted inside the case 12 adjacent the receptacle 16. A pumping member 32 of the pump engages a linearly disposed intermediate segment 34 of the disposable IV tubing apparatus 14. The pumping member 32 comprises nine individual

fingers 32a which slide back and forth toward and away from the intermediate IV tubing segment 34. fingers 32a are moved by corresponding cam wheels 36 (Fig. 6). A flexible boot 33 (Fig. 2) surrounds the 5 fingers and forms an interface between the fingers and intermediate segment 34 of IV tubing. peripheral edges of this boot are sealed to internal of the case to protect the pump contamination. Each cam wheel 36 (Fig. 5) has a 10 splined mounting hole 37 therethrough which is offset from the center of the wheel. Each finger 32a comprises a rectangular block having a circular hole in which a corresponding one of the cam wheels 36 rotates. The hole has a diameter slightly larger than 15 the outside diameter of the wheel so that the wheel can rotate inside the hole and thereby pull the finger back and forth. The motion of one of the cam wheels is illustrated in phantom lines in Fig. 6.

The cam wheels 36 are mounted on a splined shaft 20 38 in progressive, offset alignment for individually reciprocating respective ones of the fingers 32a in a predetermined, timed sequence. The linearly disposed segment 34 of IV tubing is progressively squeezed by the fingers 32a so that intravenous fluid in the 25 tubing is pumped therethrough.

The intermediate IV tubing segment 34 is preferably made of vinyl or silicone and has a maximum Durometer of seventy-five measured on the Shore A scale. By using a highly pliant, non-stiff resilient 30 flexible tubing segment of this type, it is possible for the individual fingers 32a of the peristaltic pump 30 to each squeeze off and completely close the tubing segment during one cycle of its respective cam wheel. This squeezing off is illustrated in Fig. 6. This

ensures a true positive displacement pump in which a single rotation of the splined shaft 38 will cause a predetermined volume of fluid to be pumped through the disposable IV tubing apparatus 14. Having such a 5 non-stiff disposable IV tubing apparatus 14 also ensures that less torque is required to rotate the splined shaft 38, thereby resulting in an overall reduction in energy consumption when the peristaltic pump is electrically driven from battery power as 10 hereafter described.

The fingers 32a preferably have small teats 32b (Fig. 6) projecting from the ends thereof. teats engage and squeeze the intermediate IV tubing segment 34. It has been determined that these teats 15 ensure that the tubing segment 34 will be completely squeezed off during each cycle of each finger. important to understand that the intermediate tubing segment 34 must have a minimum amount of stiffness and resilience or else it will not open and close in a to function will permit it 20 manner that peristaltic pump. Preferably the tubing segment 34 has a minimum Durometer of thirty-five measured on the Shore A scale.

Referring again to Fig. 2, the programmable for releasably 10 includes means system 25 infusion intermediate IV tubing segment mounting the adjacent the pumping member 32. The intermediate tubing segment 34 is mounted to a door 40 having a at one end and a hook-shaped member 40a (Fig. 3) 30 compressible clasp 40b other end. at the hook-shaped member 40a of the door may be engaged by the patient with a shoulder 16a (Fig. 2) located at one end of the receptacle 16 in the case 12. other end of the door is then swung in and the clasp

40b snaps into the other end of the receptacle 16. The intermediate IV tubing segment 34 is squeezed between the individual fingers 32a and a compressible, resilient pad 42 (Figs. 3 and 6) supported by the 5 innerside of the door 40. This pad may be made of polyurethane foam.

The shaft 38 (Fig. 3) which supports the cam wheels 36 is journaled at opposite ends in ball bearings 44. A gear 46 rigidly mounted on one end of the shaft 38 meshes with another gear 48 (Fig. 2) rigidly mounted on another shaft 50 of a DC motor module 51 having an internal 141:1 gear reduction. In other words, one-hundred and forty-one rotations of the armature of the DC motor turns the shaft 50 one revolution and thus the cam shaft 38 one revolution.

Referring to Fig. 4, the disposable IV tubing apparatus 14 has a proximal tubing segment 52 and a distal tubing segment 54 connected to opposite ends of the intermediate IV tubing segment 34 by means of couplings 56 and 58. These couplings are attached to the underside of the door 40 as hereafter described in conjunction with Fig. 9.

Referring to Fig. 4, the intermediate IV tubing segment 34 preferably has an inside diameter of approximately 0.125 inches. Silicone and VINYL tubing can be commercially obtained having the desired stiffness. The proximal segment 52 and the distal segment 54 are each preferably made of clear polyvinyl chloride (PVC) having an outside diameter of approximately 0.140 inches and an inside diameter of approximately .088 inches. This clear PVC tubing is larger in both inside and outside diameter than the conventional PVC tubing segments 55a and 55b (Fig. 1)

which connect the segments 52 and 54 to the spike 20 and male lure fitting 26, respectively.

prototype of our preferred actual embodiment, the designed maximum delivery rate 5 approximately three hundred milliliters per hour. minimum designed delivery rate is approximately 0.1 The delivery resolution is milliliters per hour. approximately 0.1 milliliters per hour for .01 through milliliters per hour and approximately one 10 milliliter per hour for approximately one hundred to three hundred milliliters per hour. In the prototype, the designed maximum volume to be infused (VTBI) is one thousand milliliters and the minimum volume to be infused (VTBI) is approximately 0.1 milliliters. 15 designed "keep vein open" (KVO) rate is approximately one milliliter per hour for one through three hundred milliliter per hour rates and approximately 0.1 through 0.99 milliliters per hour for 0.1 through 0.99 milliliter per hour rates.

40 Fig. 7, the door has Referring to 20 rectangular aperture 90 the formed adjacent hook-shaped member 40a. A resilient metal tubing squeezer 92 has an upper end 92a which is tightly received in the aperture 90 in the door 40. 25 squeezer 92 has a pair of parallel downwardly extending arms which terminate in coiled sections Referring to Fig. 8, when the disposable is assembled, the intermediate segment 34 is squeezed shut between the coiled sections 92b. When the door 30 40 is installed into the receptacle 16 of the case 12, the hook-shaped member 40a is engaged with the shoulder 16a (Fig. 2). The other end of the door having the clasp 40b is then swung toward the case. As this happens, the coiled sections 92b of the tubing

squeezer 92 engage upstanding projections 94 (Fig. 8) These projections are spaced so in the receptacle. that the coiled sections are displaced outwardly away from the intermediate tubing segment 34 5 unclamping the same. This is illustrated in phantom lines in Fig. 8. The squeezer performs a very important function. Namely, if the disposable IV tubing apparatus 14 should be inadvertently removed from the case 12 it will squeeze off the intermediate 10 tubing section 34 and prevent free flow intravenous fluid by gravity action.

Referring to Fig. 3, the clasp 40b consists of a V-shaped element. The door 40 is preferably made of injection molded plastic and the V-shaped clasp 40b is compressible upon swinging the clasp into the receptacle 16 in the case. This allows a wedge-shaped projection 96 on the clasp 40b to clear and snap into engagement behind an L-shaped latch 98.

Further details of the disposable 20 apparatus 14 are visible in Fig. 9. The coupling 56 is received in a slot in a bracket 102 which extends from the underside of the exterior wall of the door 40 near the clasp 40b. The coupling 56 is solvent, welded or bonded to the bracket 102. The coupling 58 25 is similarly received in another recess formed in the hook-shaped member 40a. Again the coupling 58 is solvent bonded to the member 40a. A magnet 106 (Fig. 9) is attached to the bracket 102 and detected by a Hall effect switch 108 (Fig. 3) adjacent The Hall effect switch is connected to 30 receptacle 16. the micro-controller hereafter described so that the output thereof will indicate whether or not a disposable has been correctly loaded into the case 12.

The peristaltic pump 30 is a single channel, linear peristaltic pump having nine reciprocating fingers The intermediate IV tubing segment 34 is highly flexible as previously indicated. In a preferred 5 embodiment of the disposable 14, the intermediate IV tubing segment 34 is made of silicone and has an inside diameter of approximately 0.125 inches. Approximately 0.12 milliliters of intravenous fluid are pumped through the intermediate IV tubing segment 10 34 for each single revolution of pump shaft 38. combined motor and gear reduction module 51 also preferably includes a built-in motor encoder. suitable unit is the MICRO-MO Model 1624006S. It uses (Trademark) fixotropic lubricant. TEFLON may be 15 conventional Robert's clamp 23 (Fig. provided on the segment of conventional IV tubing 55b for closing off the same.

While we have described preferred embodiments of our improved disposable infusion apparatus and 20 peristaltic pump for use therewith, it should be understood that modifications and adaptations thereof will occur to persons skilled in the art. Therefore, the protection afforded our invention should only be limited in accordance with the scope of the following 25 claims.

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CLAIMS

- 1. A disposable infusion apparatus for use with a peristaltic pump, comprising:
 - a proximal segment of IV tubing;
 - a distal segment of IV tubing;
- an intermediate segment of IV tubing having a maximum Durometer of seventy-five on the Shore A scale, the intermediate segment having a length sufficient for operative engagement with a pumping member of a peristaltic pump throughout a pumping 10 stroke thereof;
 - a first coupling connecting a first end of the proximal segment of IV tubing to a first end of the intermediate segment of IV tubing; and
- a second coupling connecting a first end of the 15 distal segment of IV tubing to a second end of the intermediate segment of IV tubing.
- 2. A disposable infusion apparatus according to Claim 1 wherein the intermediate segment of IV tubing 20 is made of a material selected from the group consisting of VINYL and silicone.
- 3. A disposable infusion apparatus according to Claim 1 wherein the intermediate segment of IV tubing 25 has a minimum Durometer of thirty-five on the Shore A scale.
- 4. A disposable infusion apparatus according to Claim 1 wherein the proximal segment of IV tubing is 30 made of polyvinyl chloride.

- 5. A disposable infusion apparatus according to Claim 1 wherein the distal segment of IV tubing is made of polyvinyl chloride.
- 6. A disposable infusion apparatus according to Claim 1 and further comprising means for releasably mounting the intermediate segment adjacent the pumping member.
- 7. A disposable infusion apparatus according to Claim 6 wherein the means for releasably mounting the intermediate segment adjacent the pumping member includes a door secured to the first and second ends of the intermediate segment of IV tubing and releasably engageable with a portion of a case defining a receptacle for positioning the intermediate segment of IV tubing in engagement with the pumping member of the peristaltic pump when it is mounted in the case adjacent the receptacle.

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- 8. A disposable infusion apparatus according to Claim 7 wherein the door has hinge means on a first end thereof for engaging the portion of the case defining the receptacle at a first end thereof for permitting a second end of the door means to swing toward and away from the case.
- 9. A disposable infusion apparatus according to Claim 8 wherein the door has clasp means on the second 30 end thereof for releasably connecting the second end of the door to the portion of the case defining the receptacle at a second end thereof.

- 10. A disposable infusion apparatus according to Claim 8 wherein the hinge means includes a hook-shaped member.
- 5 11. A disposable infusion apparatus according to Claim 8 and further comprising tube squeezer means connected to the door for normally squeezing the intermediate segment of IV tubing shut and actuable upon engagement with the case to open the intermediate 10 segment of IV tubing.
 - 12. A peristaltic pump for pumping intravenous fluid through a segment of IV tubing, comprising:

a plurality of fingers;

means for mounting the fingers in side-by-side substantially parallel relationship for individual reciprocation;

cam means for individually reciprocating respective ones of the fingers in a predetermined 20 timed sequence so that when a linearly disposed segment of IV tubing is squeezed by the fingers intravenous fluid in the tubing will be pumped therethrough; and

motor means for driving the cam means.

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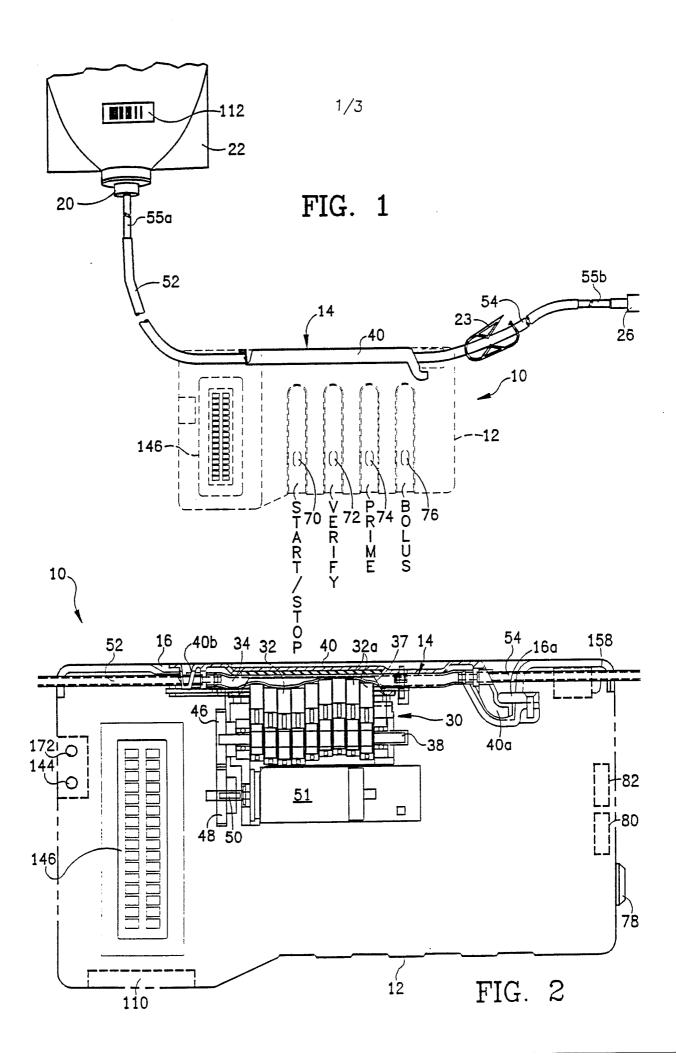
13. A peristaltic pump according to Claim 12 and further comprising a flexible boot surrounding the fingers and forming an interface between the fingers and the segment of IV tubing.

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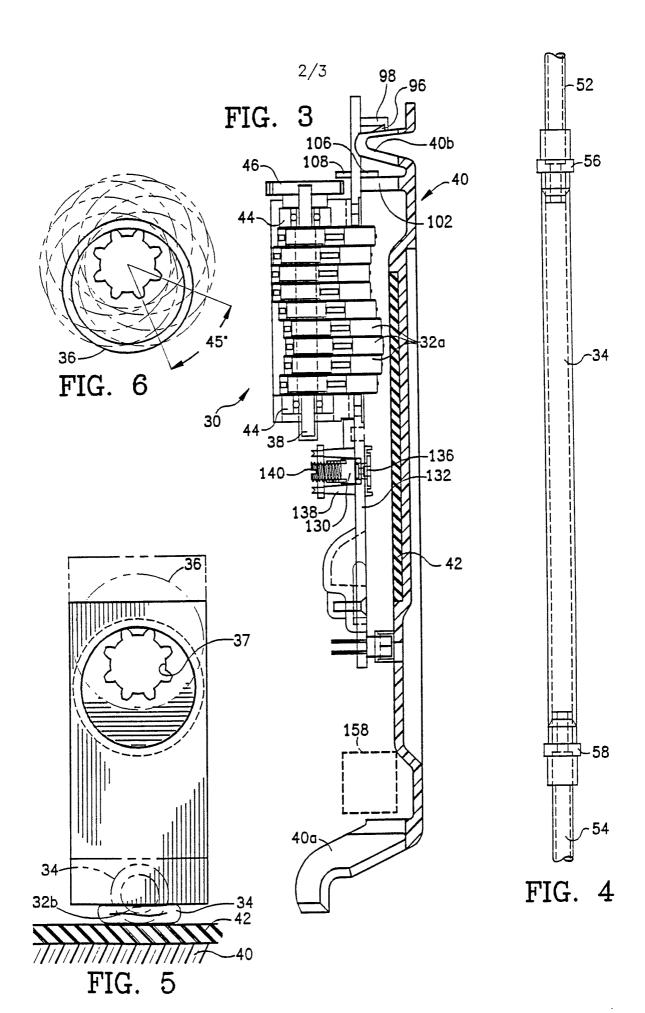
14. A peristaltic pump according to Claim 12 wherein each finger has a teat projecting therefrom for engaging the segment of IV tubing and ensuring the complete squeezing off thereof.

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wherein the cam means includes a splined shaft and a plurality of identical cam wheels, each cam wheel having a splined mounting hole therethrough offset from a center of the wheel, and the wheels being mounted on the splined shaft in progressive offset alignment for individually engaging and reciprocating respective ones of the fingers in the predetermined timed sequence.



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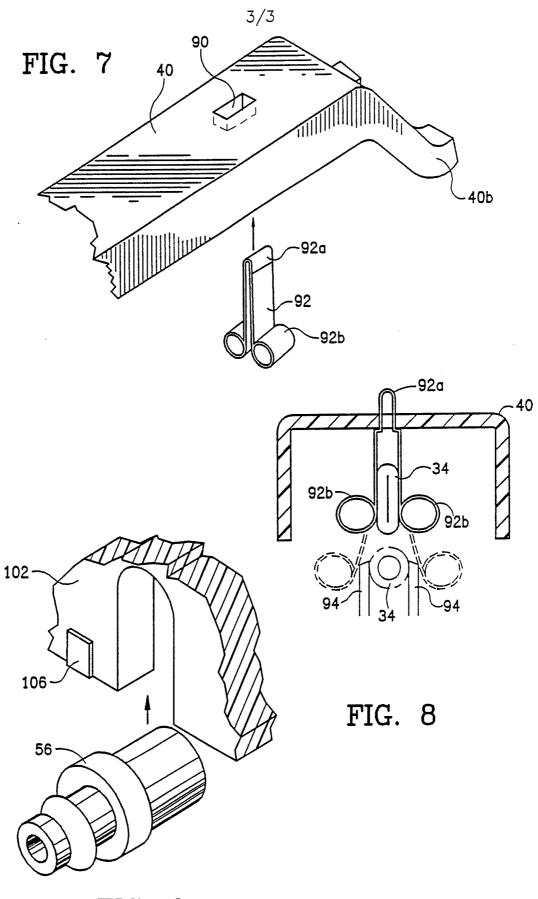


FIG. 9

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INTERNATIONAL SEARCH REPORT:

PCT/US91/02930 International Application No. I. CLASSIFICATION OF SUBJECT MATTER of several classification symbols apply indicate a Accessor (5 to internal of an Ealer be cased case of 43/08 to both National Classic cation and IPC US CT · 604/153 · 128/DTG 12 417/474

	Minimum Documentation Searchedit
lassification System	Diassification Sympols
US	604/153; 128/DIG. 12; 417/474,475,360

Y US, A, 4,493,706 (BORSANYI ET AL.) 15 JANUARY 1985 See the entire document. Y US, A, 4,997,347 (ROOS) 05 MARCH 1991 Col. 3, lines 15-18. Y US, A, 4,976,590 (BALDWIN) 11 DECEMBER 1990 Col. 8, lines 29-51. Y US, A, 4,565,542 (BERG) 21 JANAURY 1986, Col. 3, lines 27-53 and Fig. 3. A US, A, 4,653,987 (TSUJI ET AL.) 31 MARCH 1987, Col. 3, lines 40-54, Fig. 3. A US, A, 4,671,792 (BORSANYI) 09 JUNE 1987, Col. 2 lines 66-68 col. 3, lines 1-9.	Category *	Citation of Document, it with indication, where appropriate, of the relevant passages of	Relevant to Claim No	
Col. 3, lines 15-18. Y US, A, 4,976,590 (BALDWIN) 11 DECEMBER 1990 4&5 Col. 8, lines 29-51. Y US, A, 4,565,542 (BERG) 21 JANAURY 1986, 10 Col. 3, lines 27-53 and Fig. 3. A US, A, 4,653,987 (TSUJI ET AL.) 31 MARCH 1987, 7-10 Col. 3, lines 40-54, Fig. 3. US, A, 4,671,792 (BORSANYI) 09 JUNE 1987, 4&5	Y		1-10	
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- document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
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IV.	CERTIF	ICATI	ON	

Date of the Actual Completion of the International Search ²

Date of Mailing of this International Search Report 1

03 JUNE 1991

International Searching Authority 1

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Signature of Authorized Officer 10 feale fr

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FURTHER INFORMATION CONTINUED FROM THE SECOND SHEET
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V OBSERVATIONS WHERE CERTAIN CLAIMS WERE FOUND UNSEARCHABLE
This international search report has not been established in respect of certain claims under Article 17(2) (a) for the following reasons:
1 Claim numbers because they relate to subject matter i not required to be searched by this Authority, namely:
2. Claim numbers . because they relate to parts of the international application that do not comply with the prescribed require-
2. Claim numbers . because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out 1, specifically:
·
3. Claim numbers, because they are dependent claims not drafted in accordance with the second and third sentences of
PCT Rule 6.4(a).
VI. X OBSERVATIONS WHERE UNITY OF INVENTION IS LACKING?
This International Searching Authority found multiple inventions in this international application as follows:
Group I - claims 1-11, drawn to a disposable infusion apparatus IV classi-
fied in class 604, subclass 153.
Group II - claims 12-15, drawn to a peristaltic pump classified in class
417. Subclass 474. 1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims
of the international application.
2. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only
those claims of the international application for which fees were paid, specifically claims:
3. X No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to
the invention first mentioned in the claims; it is covered by claim numbers: 1-11
4. As all searchable claims could be searched without effort justifying an additional fee, the International Searching Authority did not invite payment of any additional fee.
Remark on Protest
The additional search fees were accompanied by applicant's protest.
No protest accompanied the payment of additional search fees.
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