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(71) **Applicant (for all designated States except US):** KONINKLIJKE PHILIPS ELECTRONICS N.V. [NL/NL]; Groenewoudseweg 1, NL-5621 BA Eindhoven (NL).

(72) **Inventors; and**

(75) **Inventors/Applicants (for US only):** LIN, Wei [CN/US]; c/o High Tech Campus Building 44, NL-5656 AE Eindhoven (NL). HUANG, Feng [US/US]; c/o High Tech Campus Building 44, NL-5656 AE Eindhoven (NL).

(74) **Agents:** VAN VELZEN, Maaïke, M. et al.; High Tech Campus 44, NL-5600 AE Eindhoven (NL).

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Declarations under Rule 4.17:

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(54) **Title:** MRI METHOD FOR RETROSPECTIVE MOTION CORRECTION WITH INTERLEAVED RADIAL ACQUISITION

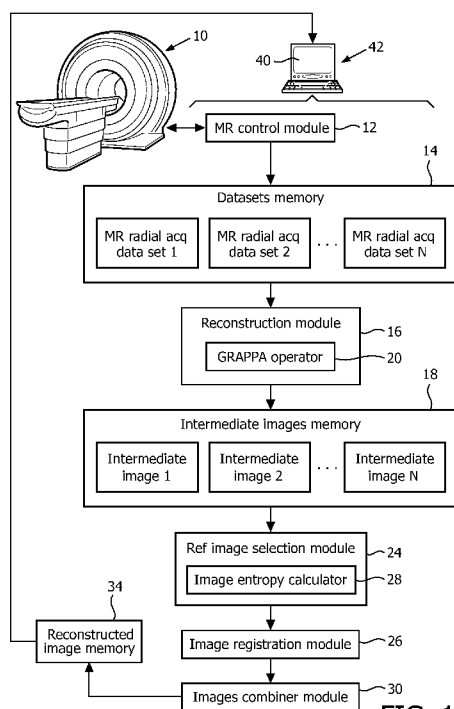


FIG. 1

(57) **Abstract:** A motion-corrected magnetic resonance imaging method comprises: sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner; reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images, the reconstructing including expanding radial k-space lines of the magnetic resonance radial acquisition dataset into corresponding radial bands in k-space using a generalized auto-calibrating partially parallel acquisition (GRAPPA) operator; selecting a reference image from the set of images; performing three-dimensional spatial registration of each image of the set of images except the reference image with respect to the reference image to generate a spatially registered set of images; and combining the spatially registered set of images to generate a motion corrected image.



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- *as to applicant's entitlement to apply for and be granted a patent (Rule 4.17(ii))*
- *as to the applicant's entitlement to claim the priority of the earlier application (Rule 4.17(iii))*
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- *with international search report (Art. 21(3))*
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MRI METHOD FOR RETROSPECTIVE MOTION CORRECTION WITH INTERLEAVED RADIAL ACQUISITION

DESCRIPTION

The following relates to the magnetic resonance imaging arts, medical imaging arts, and related arts.

Three-dimensional magnetic resonance (MR) imaging of a human or other animate subject can provide useful information. Such imaging is used for medical or veterinary diagnosis, for medical or veterinary clinical analysis, for monitoring or assessment of a known medical or veterinary condition in a subject, for medical or veterinary screening tasks, and so forth. However, subject motion can be a problem in the case of animate subjects. Likelihood of subject motion increases with increasing time duration of the MR data acquisition.

A three dimensional imaging dataset can be acquired by either performing multi-slice imaging in which the acquisition of a plurality of spaced-apart parallel slices are interleaved into a single MR excitation repeat time (TR). Alternatively, a three dimensional imaging dataset can be acquired by employing a slice-encoding inner loop. In either case, the imaging data are organized into slices, and the subject motion may be either in the "in-slice" plane, or may be "through-plane" motion in a direction generally transverse to the slices. In-slice motion can sometimes be compensated by shifting or rotating imaging data acquired after a motion event. Data affected by through-plane motion is generally discarded. However, in some application such as head imaging, substantial through-plane motion is a relatively common occurrence, and discarding data affected by such through-plane motion is problematic.

Radial imaging is sometimes employed to facilitate motion correction. Radial imaging provides a "built-in" oversampling of central k-space region, which can be used to assess data-consistency, to provide self-gating, and for correcting rigid or non-rigid subject motion. However, there is a tradeoff between temporal resolution and robustness for radial motion correction, in that more radial lines enhance robustness of the motion correction but reduce temporal resolution for the motion correction.

The following provides new and improved apparatuses and methods as disclosed herein.

In accordance with one disclosed aspect, a method comprises: sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner; reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images; spatially registering the set of images; and combining the spatially registered set of images to generate a motion corrected image.

In accordance with another disclosed aspect, a method comprises: sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner; reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images, the reconstructing including expanding radial k-space lines of the magnetic resonance radial acquisition dataset into corresponding radial bands in k-space using a generalized auto-calibrating partially parallel acquisition (GRAPPA) operator; selecting a reference image from the set of images; performing three-dimensional spatial registration of each image of the set of images except the reference image with respect to the reference image to generate a spatially registered set of images; and combining the spatially registered set of images to generate a motion corrected image.

In accordance with another disclosed aspect, a method comprises: sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner; reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images; selecting a reference image from the set of images as the image having lowest entropy; performing spatial registration of each image of the set of images except the reference image with respect to the reference image to generate a spatially registered set of images; and combining the spatially registered set of images to generate a motion corrected image.

In accordance with another disclosed aspect, a method as set forth in any one of the three immediately preceding paragraphs is disclosed, further comprising displaying or printing the motion-corrected image. In accordance with another disclosed aspect, a method as set forth in any one of the three immediately preceding paragraphs is disclosed, wherein the reconstructing, spatial registering, and combining are performed by a digital processor. In accordance with another disclosed aspect, a digital processor

configured to perform a method as set forth in any one of the three immediately preceding paragraphs is disclosed. In accordance with another disclosed aspect, a storage medium is disclosed storing instructions executable by a digital processor to perform a method as set forth in any one of the three immediately preceding paragraphs.

5 One advantage resides in improved motion compensation in MR images.

Another advantage resides in faster acquisition of motion compensated MR images.

Another advantage resides in providing for retrospective tradeoff between motion correction robustness and temporal resolution.

10 Further advantages will be apparent to those of ordinary skill in the art upon reading and understanding the following detailed description.

FIGURE 1 diagrammatically shows an imaging system configured to perform motion-corrected magnetic resonance imaging.

15 FIGURE 2 diagrammatically shows a motion-corrected magnetic resonance imaging method suitably performed by the imaging system of FIGURE 1.

FIGURE 3 diagrammatically shows a set of four interleaved magnetic resonance radial acquisition datasets and the resulting combined dataset.

FIGURE 4 diagrammatically shows a set of two interleaved magnetic resonance radial acquisition datasets and the resulting combined dataset.

20 FIGURE 5 diagrammatically shows a magnetic resonance radial acquisition dataset with an indication of the region within which the Nyquist criterion is satisfied.

25 FIGURE 6 diagrammatically shows the magnetic resonance radial acquisition dataset of FIGURE 5 after expanding each radial k-space line into a radial band in k-space using a generalized auto-calibrating partially parallel acquisition (GRAPPA) operator, with an indication of the region within which the Nyquist criterion is satisfied.

FIGURE 7 diagrammatically shows the GRAPPA extrapolation used to convert the data of FIGURE 5 to the data of FIGURE 6.

30 FIGURE 8 diagrammatically shows a plurality of spaced-apart regions of interest at each of which relative motion between the image and the reference image is determined in order to perform motion correction.

With reference to FIGURES 1 and 2, an imaging system and method, respectively, are shown for performing motion-corrected imaging. The imaging system includes a magnetic resonance (MR) scanner **10**, such as an illustrated AchievaTM MR scanner (available from Koninklijke Philips Electronics N.V., Eindhoven, The Netherlands), or an InteraTM or PanoramaTM MR scanner (both also available from Koninklijke Philips Electronics N.V.), or another commercially available MR scanner, or a non-commercial MR scanner, or so forth. In a typical embodiment, the MR scanner includes internal components (not illustrated) such as a superconducting or resistive main magnet generating a static (B_0) magnetic field, sets of magnetic field gradient coil windings for superimposing selected magnetic field gradients on the static magnetic field, a radio frequency excitation system for generating a radiofrequency (B_1) field at a frequency selected to excite magnetic resonance (typically ^1H magnetic resonance, although excitation of another magnetic resonance nuclei or of multiple magnetic resonance nuclei is also contemplated), and a radio frequency receive system including a radio frequency receive coil array, or a plurality of receive coils, for detecting magnetic resonance signals emitted from the subject.

In an magnetic resonance (MR) acquisition operation **S1** (see FIGURE 2), the MR scanner **10** is controlled by a magnetic resonance (MR) control module **12** to sequentially acquire a plurality of interleaved magnetic resonance (MR) radial acquisition datasets which are stored in a datasets memory **14**. Without loss of generality, the number of acquired MR radial acquisition datasets is denoted as N where N is a positive integer greater than one. Each MR radial acquisition dataset includes n radial k-space lines and has n -fold rotational symmetry in k-space, where n is a positive integer greater than one. The plurality of interleaved MR radial acquisition datasets thus includes $N \times n$ radial k-space lines, and the interleaving is selected such that this combined set of $N \times n$ radial k-space lines has $N \times n$ fold rotational symmetry in k-space where N is a positive integer greater than one. The disclosed acquisition **S1** employs partial parallel imaging (PPI), and accordingly a plurality (i.e., two or more) receive coils are employed in the acquisition **S1**.

With continuing reference to FIGURES 1 and 2 and with further reference to FIGURE 3, an illustrative example of the acquisition operation **S1** is shown, in which the number of interleaved MR radial acquisition datasets is $N=4$, with each MR radial acquisition dataset including $n=4$ radial k-space lines. (As used herein, a "radial k-space

line" is considered to extend outward from the center of k-space or, alternatively, to begin at a periphery of k-space and extend radially inward to the center of k-space.) The four interleaved MR radial acquisition datasets of illustrative FIGURE 3 are denoted by binary notation: MR radial acquisition set "00" is acquired first; MR radial acquisition set "01" is acquired second; MR radial acquisition set "10" is acquired third; and MR radial acquisition set "11" is acquired last. Each MR radial acquisition set has four-fold (i.e., n-fold) rotational symmetry in k-space, while the combined interleaved MR radial acquisition dataset (shown on the righthand side of FIGURE 3) has sixteen-fold (i.e., $N \times n$ -fold) rotational symmetry in k-space. This illustrative example is an interleaved or "bit-reverse" acquisition scheme.

Because the four interleaved MR radial acquisition datasets are acquired in the order: "00", "01", "10", "11", it follows that subject motion will produce blurring only in the dataset or datasets during which the motion occurs. Additionally, any dataset acquired after a motion event will (in general) have some spatial misalignment as compared with the dataset(s) acquired before the motion event.

With continuing reference to FIGURE 3 and with further reference to FIGURE 4, by suitable selection of the order of acquisition of the interleaved MR radial acquisition datasets, it is possible to have various groupings of the datasets to provide a retrospective tradeoff between temporal resolution and motion correction robustness. In FIGURE 4, the four interleaved MR radial acquisition datasets are grouped into two interleaved MR radial acquisition datasets. Toward this end, the first two acquired datasets "00" and "01" are grouped as a single MR radial acquisition dataset "0" and the second two (subsequently acquired) datasets "10" and "11" are grouped as a single MR radial acquisition dataset "1". Thus, in the case of FIGURE 4, $N=2$ and each MR radial acquisition dataset has $n=8$ radial k-space lines and 8-fold rotational symmetry in k-space, while the combined dataset (shown on the righthand side of FIGURE 3) has $N \times n = 2 \times 8 = 16$ radial k-space lines. The result of the grouping of FIGURE 4 (as compared with the grouping of FIGURE 3) is more robust motion correction due to the larger number of radial k-space lines ($n=8$ in FIGURE 4 as compared with $n=4$ in FIGURE 3) but poorer temporal resolution due to the fewer number of interleaved datasets ($N=2$ in FIGURE 4 as compared with $N=4$ in FIGURE 3).

With returning reference to FIGURES 1 and 2 and with further reference to FIGURE 5, in an operation **S2** each of the N interleaved MR radial acquisition datasets is reconstructed by a reconstruction processor **16**. This results in generation of N (intermediate) images, which are suitably stored in an intermediate images memory or buffer **18**. To enhance temporal resolution, in the illustrative embodiments each MR radial acquisition dataset is undersampled, that is, contains fewer radial k-space lines than would be needed to construct a full image. FIGURE 5 diagrammatically denotes this undersampling by showing the combined interleaved MR radial acquisition dataset with a "Nyquist circle" N_{acq} denoting the central k-space region within which the Nyquist criterion is satisfied. Data outside the Nyquist circle N_{acq} is undersampled.

With continuing reference to FIGURES 1, 2, and 5, and with further reference to FIGURES 6 and 7, to accommodate the undersampling, the illustrative reconstruction processor **16** includes implementation of a GRAPPA operator **20** which is applied to expand each radial k-space line into a radial band in k-space. The acronym "GRAPPA" stands for "generalized auto-calibrating partially parallel acquisition". GRAPPA is a partial parallel imaging (PPI) technique that utilizes information provided by simultaneous data acquisition using a plurality of receive elements (e.g., receive coils) with different coil sensitivities to extrapolate acquired k-space data. In the reconstruction operation **S2**, the GRAPPA operator **20** is used to expand each acquired radial k-space line into a radial band in k-space, as diagrammatically illustrated in FIGURE 6. This usage of GRAPPA is also known in the art as the GRAPPA Operator for Wider Radial band ("GROWL") algorithm. Lin et al., "GRAPPA Operator for Wider RadiaL Band (GROWL)", Proc. Intl. Soc. Mag. Reson. Med. 17, page 4553 (2009). In the GROWL algorithm, the GRAPPA operator **20** is used to widen each radial k-space line into a radial band in k-space consisting of several parallel lines, followed by a suitable regridding procedure. *Id.* This results in an enlarged Nyquist circle N_{GROWL} which is the central k-space region within which the Nyquist criterion is satisfied by the radial bands in k-space. The k-space data within the initial Nyquist circle N_{acq} is used for self-calibration, and is suitably rotated to a Cartesian grid. *Id.* FIGURE 7 diagrammatically shows the process for a single radial k-space line **L**: the calibration is first performed in the (initial) Nyquist circle N_{acq} , followed by GRAPPA extrapolation from the acquired k-space

samples (indicated in FIGURE 7 by filled black circles lying on the radial k-space line **L**) to target extrapolated k-space samples (indicated in FIGURE 7 by open circles).

In correspondence with the source datasets, subject motion will produce blurring only in the (intermediate) image or images whose dataset was (were) acquired during the motion. Additionally, any image whose dataset was acquired after a motion event will (in general) have some spatial misalignment as compared with image(s) whose dataset(s) was (were) acquired before the motion event. However, such misalignment can be compensated by rigid or non-rigid spatial registration.

With continuing reference to FIGURES 1 and 2, toward this end a reference image selection module **24** selects a reference image from the set of (intermediate) images in an operation **S3**, and an image registration module **26** spatially registers each image of the set of (intermediate) images except the reference image with the reference image in an operation **S4** to generate a spatially registered set of images. Said another way, the reference image selection module **24** selects a reference image from the N images in the operation **S3**, and the image registration module **26** spatially registers each of the remaining (N-1) images of the set of images with the reference image in the operation **S4**.

The operation **24** preferably selects a reference image that is not affected, or is minimally affected, by subject motion. In the illustrative embodiment, this is achieved by including an image entropy calculator **28** in the reference image selection module **24**, and selecting the reference image as the image having lowest entropy. The principle behind this approach is that motion blurring due to subject motion during acquisition of the MR radial acquisition dataset is generally expected to increase the image entropy in the corresponding reconstructed image.

With continuing reference to FIGURES 1 and 2 and with further reference to FIGURE 8, the image registration module **26** can employ substantially any image registration technique in performing the image registration operation **S4**. In a suitable embodiment diagrammatically shown in FIGURE 8, each of the (N-1) images is spatially registered with the reference image in three dimensions. As between a given image and the reference image, the relative motion equals the misalignment between the image and the reference image. As diagrammatically shown in FIGURE 8, with both in-plane relative motion and through-plane relative motion are determined at each of a plurality of spaced-apart regions of interest, namely three regions of interest (ROI) **R₁**, **R₂**, **R₃** in the

illustrative example of FIGURE 8. In FIGURE 8, the three regions of interest (ROI) R_1 , R_2 , R_3 are shown both in an axial slice of an illustrative head image (lefthand side of FIGURE 8) and in a diagrammatic perspective view (righthand side of FIGURE 8). Although three ROI R_1 , R_2 , R_3 are shown in the illustrative example, more or fewer ROI
5 can be used in assessing image misalignment. The number and locations of the ROI should be selected so as to detect most likely rigid and non-rigid subject motions.

In a suitable image correlation method for the motion detection, a two-dimensional correlation between the image and the reference image is determined in image space, and the maximal correlation then yields both detected rotation and translation.

10 Image correlation advantageously can be computed rapidly in k-space. To account for potentially large rotation within each ROI R_1 , R_2 , R_3 , the reference image may optionally be pre-rotated in-plane to various angles prior to the image correlation, and the pre-rotation yielding the best image correlation is then the determined rotation. The detected rotation is suitably corrected by the image registration module 26 in the operation S4 by modifying
15 the radial trajectories, while translational motion is suitably corrected by applying the corresponding linear phase term. The output of the operations S3, S4 is a set of registered (intermediate) images.

With continuing reference to FIGURES 1 and 2, the set of registered (intermediate) images are combined by an images combiner module 30 to form a
20 motion-corrected image in an operation S5. The motion-corrected image is suitably stored in a reconstructed image memory 34, and is optionally displayed on the display 40 of a computer 42, and/or printed using a suitable printing device, and/or communicated via the Internet or a local medical network, or otherwise utilized.

In the illustrated embodiment, control and data processing modules 12, 16,
25 24, 26, 28 and memories 14, 18, 34 are embodied by the illustrative computer 42 whose processor (which include one or more of a multi-core processor or other parallel processing digital processing device, a single-core processor, a graphical processing unit (GPU), or so forth) is programmed to implement the control and processing functions of the modules 12, 16, 24, 26, 28 and which has a hard drive, optical drive, random access memory (RAM), or
30 other storage medium implementing the memories 14, 18, 34 and/or storing instructions executable by the computer to perform the control and processing functions of the modules 12, 16, 24, 26, 28. The illustrative computer 42 also has the illustrative display 40 for

displaying MR images and other visual information. In other embodiments, a dedicated MR controller, MR reconstruction system, or other digital device or devices is employed to embody the processing and/or storage **12, 14, 16, 18, 24, 26, 28, 34.**

The disclosed motion-corrected imaging techniques have been implemented
5 in an illustrative *in vivo* motion corrected head imaging experiment. In this experiment, a healthy volunteer was scanned on a 3.0T Achieva™ MR scanner using an eight-channel head coil (available from Invivo, Gainesville, FL) and a multi-slice two-dimensional radial gradient echo sequence. A bit-reversed acquisition sequence as per FIGURE 3 was employed (but not necessarily with the same values of n and N as in FIGURE 3). As noted
10 with reference to FIGURE 4, the bit-reversed scheme provides flexibility in choosing an appropriate temporal resolution retrospectively. Scan parameters were as follows: FOV 230×230 mm², slice thickness 5 mm, matrix size 256 (readout) $\times$ 256 (view no.), TR/TE=250/6.9 ms, flip angle = 800. To generate a motion-corrupted dataset, the subject was asked to perform head-shaking several times during the scan. Data were grouped into
15 interleaves based on the acquisition order, and GROWL reconstruction as per operation **S2** was carried out for each interleaf. The interleaf having lowest image entropy value was chosen as the reference as per operation **S3**, and the two-dimensional rotation/translation was detected using the image correlation method as per operation **S4**. The detected rotation was then used to modify the radial trajectories, while translational motion was corrected by
20 applying the corresponding linear phase term. These experiments indicate that the disclosed motion-corrected imaging approaches are suitably used for head imaging using as few as 16 radial lines (that is, $N \times n = 16$). Motion trajectory detected from the two-dimensional image correlation shows both continuous and abrupt components, with a rotation range of 5.5° and a translation range of 5 pixels. The entire motion detection and
25 correction procedure took about 20 seconds for these experiments.

This application has described one or more preferred embodiments. Modifications and alterations may occur to others upon reading and understanding the preceding detailed description. It is intended that the application be construed as including all such modifications and alterations insofar as they come within the scope of the
30 appended claims or the equivalents thereof.

CLAIMS

Having thus described the preferred embodiments, the invention is now claimed to be:

1. A method comprising:
sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner;
reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images;
spatially registering the set of images; and
combining the spatially registered set of images to generate a motion-corrected image.
2. The method as set forth in claim 1, wherein:
each magnetic resonance radial acquisition dataset includes n radial k-space lines and has n -fold rotational symmetry in k-space where n is a positive integer greater than one, and
the plurality of interleaved magnetic resonance radial acquisition datasets comprises N interleaved radial acquisition datasets and includes $N \times n$ radial k-space lines and has $N \times n$ fold rotational symmetry in k-space where N is a positive integer greater than one.
3. The method as set forth in claim 2, wherein n is an even integer.
4. The method as set forth in claim 1, wherein the reconstructing of each magnetic resonance radial acquisition dataset comprises:
expanding each radial k-space line into a radial band in k-space using partial parallel imaging (PPI).
5. The method as set forth in claim 1, wherein the reconstructing of each magnetic resonance radial acquisition dataset comprises:

expanding each radial k-space line into a radial band in k-space using a generalized auto-calibrating partially parallel acquisition (GRAPPA) operator.

6. The method as set forth in claim 1, wherein the reconstructing of each magnetic resonance radial acquisition dataset comprises:

reconstructing the magnetic resonance radial acquisition dataset using the GRAPPA operator for wider radial band (GROWL) algorithm.

7. The method as set forth in claim 1, wherein the spatial registering comprises:

selecting a reference image from the set of images; and
spatially registering each image of the set of images except the reference image with the reference image to generate a spatially registered set of images.

8. The method as set forth in claim 7, wherein the selecting comprises:
selecting the reference image as the image having lowest entropy.

9. The method as set forth in claim 7, wherein the spatial registering of each image of the set of images with the reference image comprises:

determining relative motion between the image and the reference image at each of a plurality of spaced-apart regions of interest.

10. The method as set forth in claim 9, wherein the relative motion between the image and the reference image at each region of interest is determined using image correlation.

11. The method as set forth in claim 7, wherein the spatial registering of each image of the set of images with the reference image comprises:

spatially registering the image with the reference image in three dimensions.

12. The method as set forth in claim 1, wherein the combining comprises:

additively combining the spatially registered set of images in image space to generate the motion-corrected image.

- 13.** The method as set forth in claim **1**, further comprising:
displaying or printing the motion-corrected image.
- 14.** The method as set forth in claim **1**, wherein the reconstructing, spatial registering, and combining are performed by a digital processor.
- 15.** A digital processor configured to perform a method as set forth in claim **1**.
- 16.** A storage medium storing instructions executable by a digital processor to perform a method as set forth in claim **1**.
- 17.** A method comprising:
sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner;
reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images, the reconstructing including expanding radial k-space lines of the magnetic resonance radial acquisition dataset into corresponding radial bands in k-space using a generalized auto-calibrating partially parallel acquisition (GRAPPA) operator;
selecting a reference image from the set of images;
performing three-dimensional spatial registration of each image of the set of images except the reference image with respect to the reference image to generate a spatially registered set of images; and
combining the spatially registered set of images to generate a motion-corrected image.
- 18.** The method as set forth in claim **17**, wherein the performing of three-dimensional spatial registration of each image comprises:
determining three-dimensional motion by regional correlation applied to a plurality of regions of interest.
- 19.** A method comprising:

sequentially acquiring a plurality of interleaved magnetic resonance radial acquisition datasets using a magnetic resonance scanner;

reconstructing each magnetic resonance radial acquisition dataset into a corresponding image to generate a set of images;

selecting a reference image from the set of images as the image having lowest entropy;

performing spatial registration of each image of the set of images except the reference image with respect to the reference image to generate a spatially registered set of images; and

combining the spatially registered set of images to generate a motion-corrected image.

20. The method as set forth in claim **19**, wherein the reconstructing includes expanding radial k-space lines of the magnetic resonance radial acquisition dataset into corresponding radial bands in k-space using a generalized auto-calibrating partially parallel acquisition (GRAPPA) operator.

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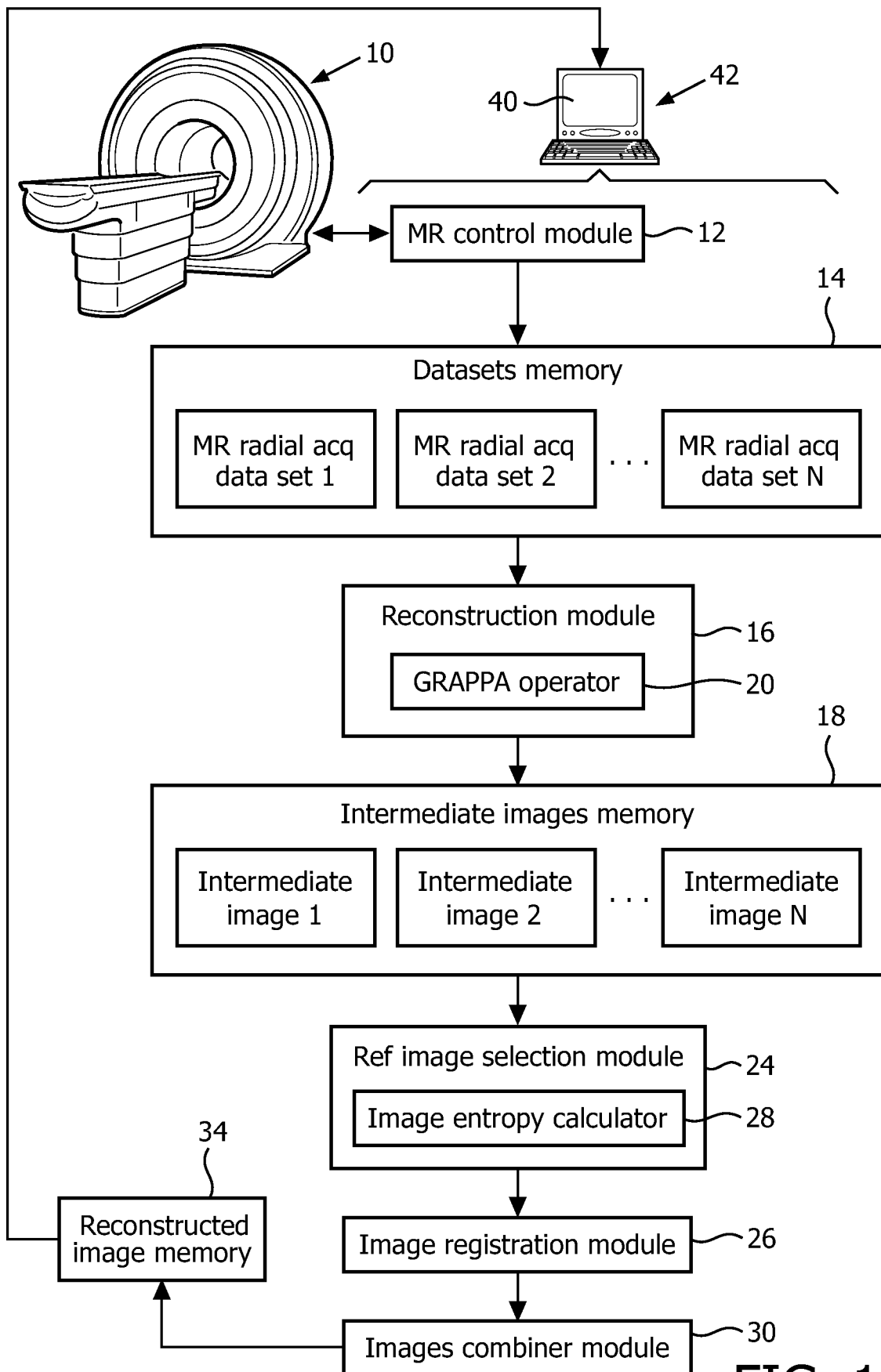


FIG. 1

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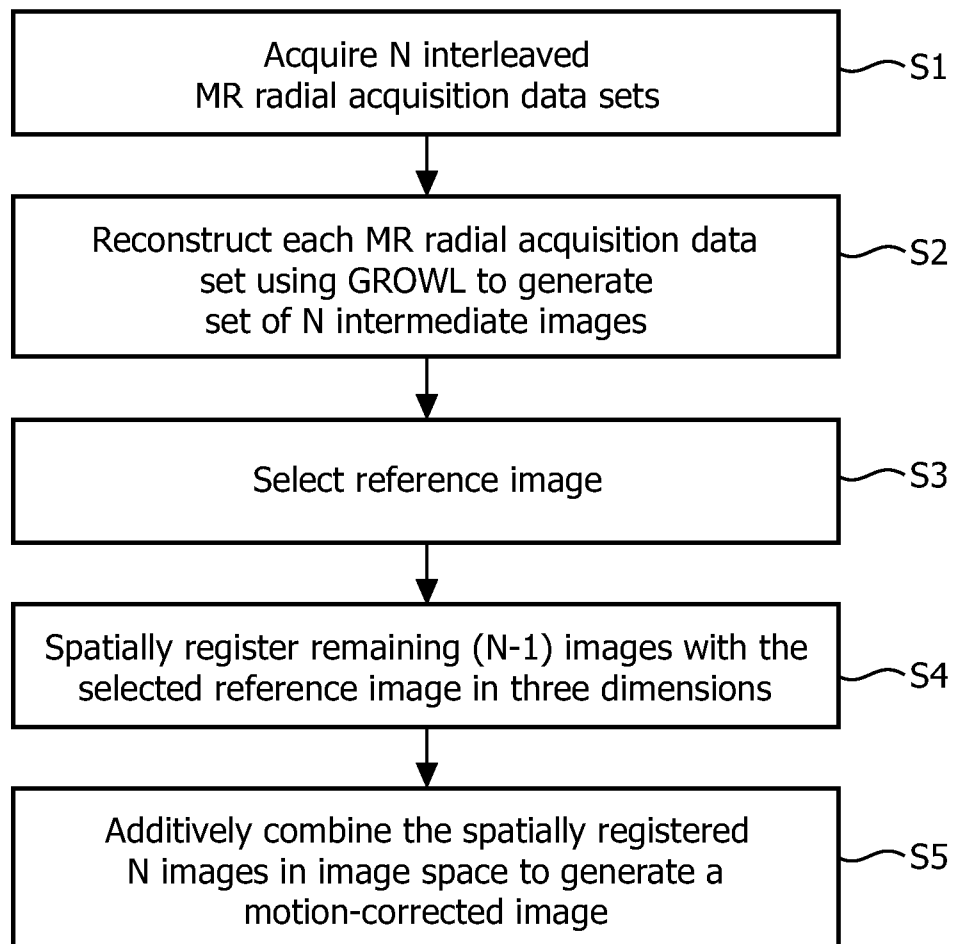


FIG. 2

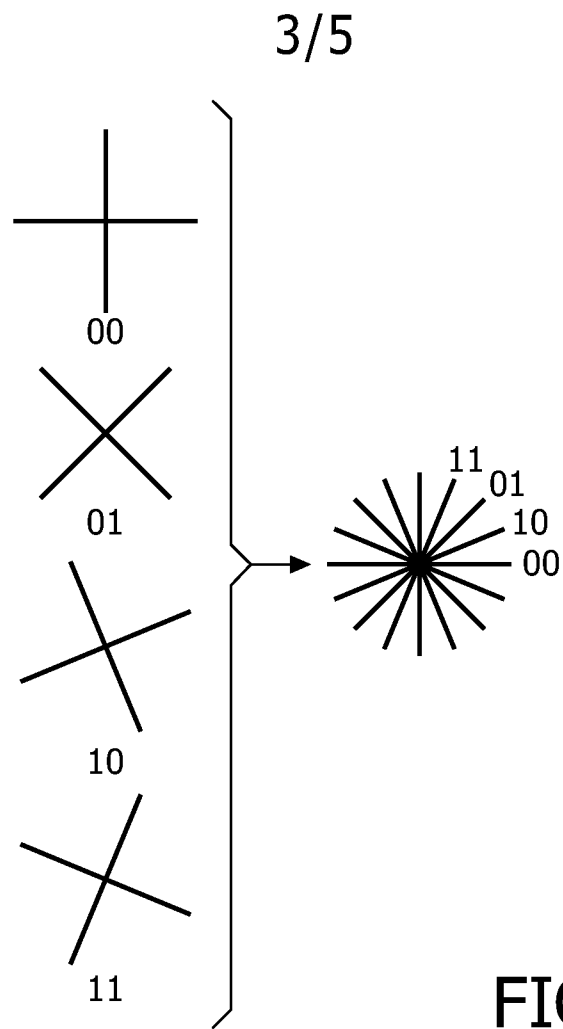


FIG. 3

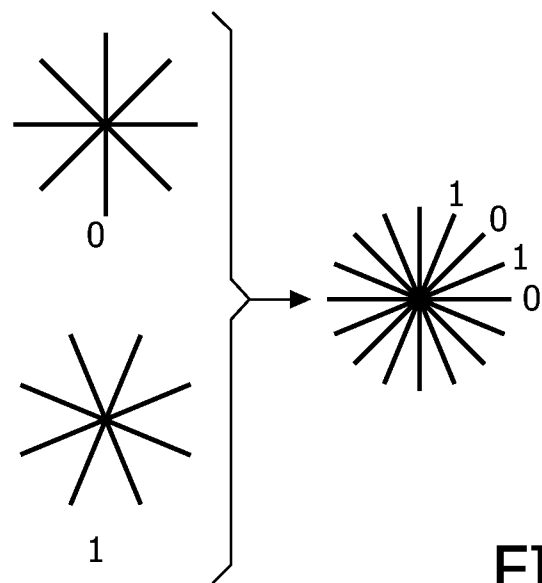


FIG. 4

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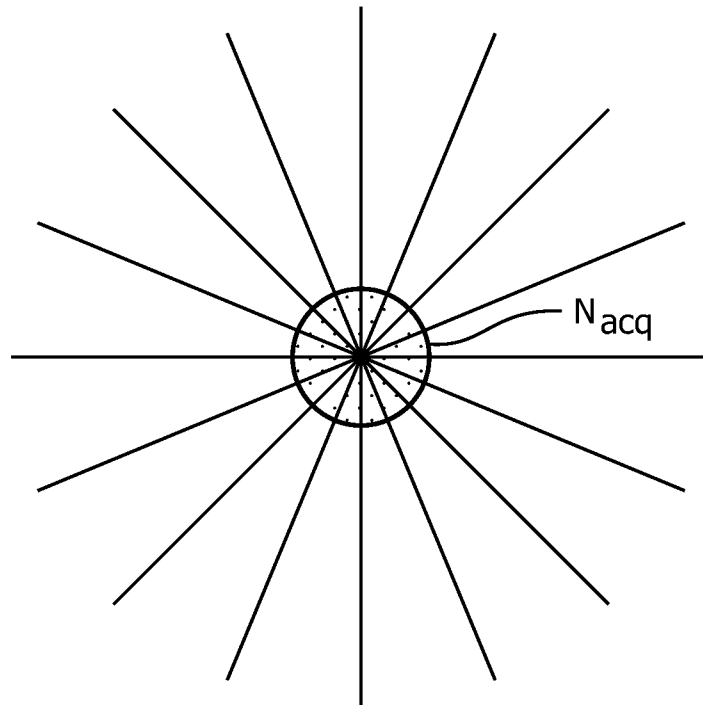


FIG. 5

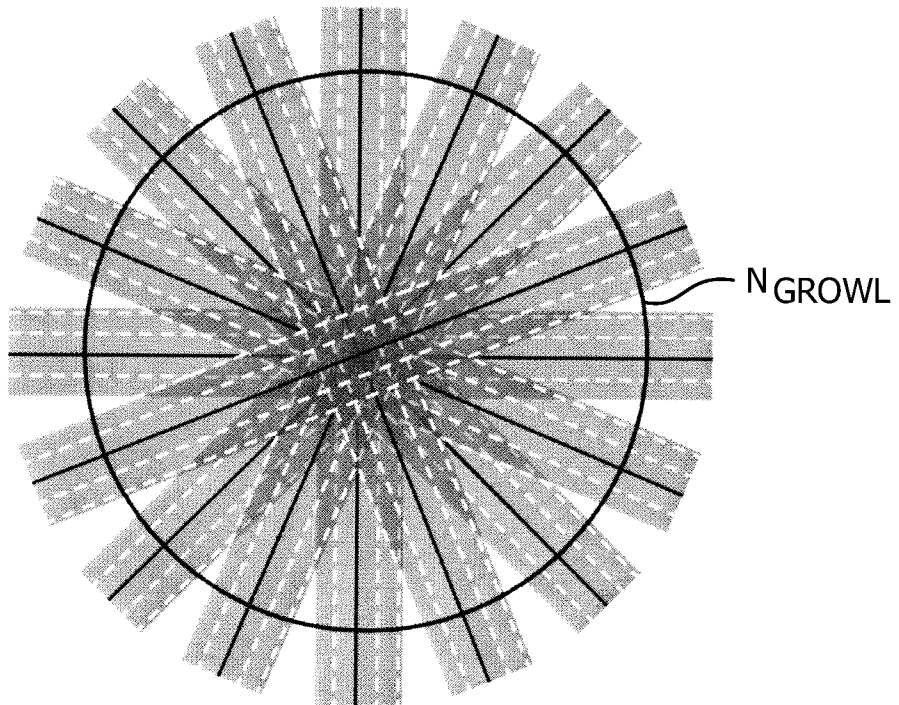


FIG. 6

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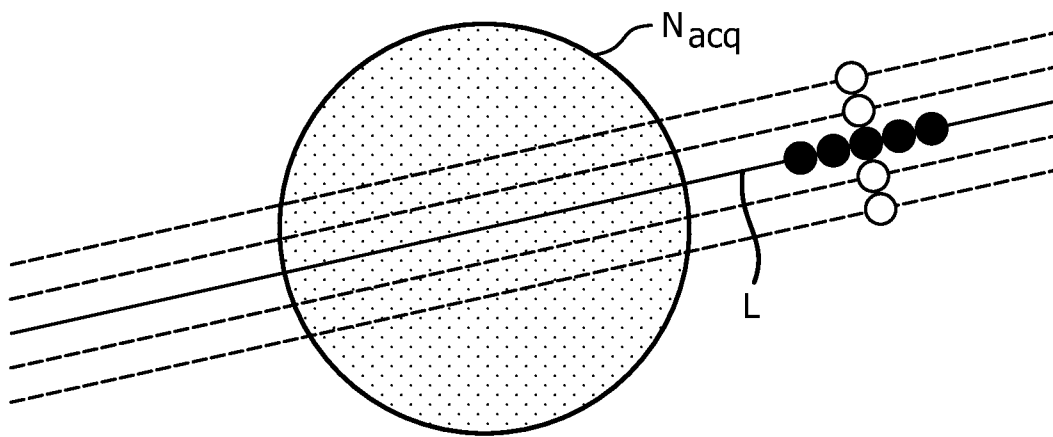


FIG. 7

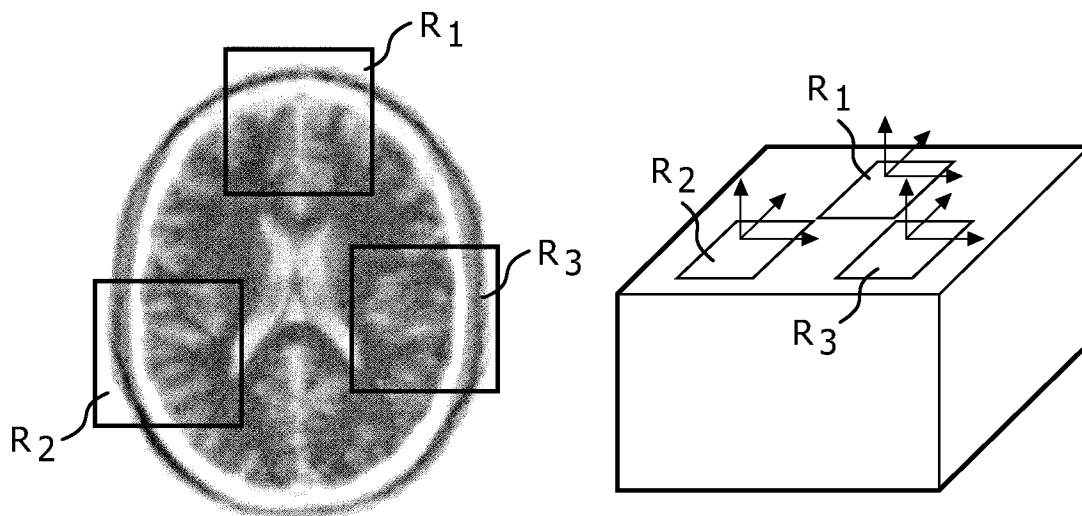


FIG. 8

INTERNATIONAL SEARCH REPORT

International application No
PCT/IB2011/053251

A. CLASSIFICATION OF SUBJECT MATTER

INV. G01R33/561 G01R33/565 G01R33/48
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
G01R

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	STEFAN SKARE ET AL: "An auto-calibrated, angularly continuous, two-dimensional GRAPPA kernel for propeller trajectories", MAGNETIC RESONANCE IN MEDICINE, vol. 60, no. 6, 24 November 2008 (2008-11-24), pages 1457-1465, XP55012933, ISSN: 0740-3194, DOI: 10.1002/mrm.21788	1,4,5, 7-20
Y	page 1458 - page 1461; figures 1-5 ----- -/--	4,5,17, 20



Further documents are listed in the continuation of Box C.



See patent family annex.

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Date of the actual completion of the international search

24 November 2011

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Name and mailing address of the ISA/

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040,
Fax: (+31-70) 340-3016

Authorized officer

Raguin, Guy

INTERNATIONAL SEARCH REPORT

International application No

PCT/IB2011/053251

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
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X	----- KIM ET AL: "Automatic correction of in-plane bulk motion artifacts in self-navigated radial MRI", MAGNETIC RESONANCE IMAGING, ELSEVIER SCIENCE, TARRYTOWN, NY, US, vol. 26, no. 3, 20 February 2008 (2008-02-20), pages 367-378, XP022511973, ISSN: 0730-725X, DOI: 10.1016/J.MRI.2007.05.007	1-3, 7-16,19
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International application No
PCT/IB2011/053251

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

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