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DESCRIPTION

FIELD OF THE INVENTION

[0001] The present invention relates to computerized modeling of three-dimensional objects, and, more particularly, to a system and method for three-dimensional modeling of intra-oral objects and features in dental applications.

BACKGROUND OF THE INVENTION

[0002] There is a need in dental medicine for making three dimensional (herein also denoted as "3D") models of internal scenes of the mouth. The term "intra-oral scene" herein denotes any collection of intra-oral objects, artifacts, surfaces, or features which can be visualized and modeled. Such models of intra-oral scenes can support various aspects of dental practice. A well-known illustration of the utility, effectiveness, and procedural and economic impact of automatic measuring and imaging techniques in dentistry involves the examination, charting, diagnosing, and treatment of dental patients who require prostheses such as crowns, bridges, dentures, or implants. Data and information obtained from measuring, imaging, and mapping intra-oral objects can be used to accurately and cost-effectively design, manufacture, fit, and monitor dental prostheses, thereby replacing currently-used inaccurate non-imaging techniques, which are labor-intensive and otherwise costly in materials and time. Automatic dental measuring and imaging techniques are also applicable for performing various types of restorative procedures, occlusal registration, and orthodontic and temporomandibular joint (TMJ) dysfunction therapies.

[0003] Electro-optical techniques are often used in medical imaging because they are relatively inexpensive in capital outlay as well as in cost-per-use, and are perceived as being non-harmful to the patient. Such techniques, however, must be adapted to the particular circumstances and problems associated with dental imaging.

[0004] Important constraints in applying medical optical imaging to the dental field include:

- space limitations -equipment must be compact enough to fit comfortably within the confines of the mouth;
- time limitations - the image must be formed in a brief time to avoid problems of the movement of the patient as well as the movement of the practitioner and apparatus; and
- surface detail limitations - accurately plotting 3D surface contours of intra-oral scenes must take into account the absence or paucity of surface detail in many close-up applications, where only partial views of intra-oral features may be available.

[0005] Measuring the three-dimensional distribution and mapping of intra-oral objects, has been implemented by using various methods. Typical intra-oral objects and features include, but are not limited to a part or entirety of any combination of: teeth; gum; intra-oral soft tissue; bone matter; dental undercuts; dental fixtures and dental prostheses of any kind, permanent or removable, which are located inside the oral cavity. Specific intra-oral objects and features can be measured, for example, as disclosed in U.S. Patent 6,402,707 to Ernst, one of the present inventors, pertaining chiefly to dental applications. In the present application, many well-known methods can be used for producing a compound database which can be stored in a computer to serve as reference for consequent medical procedures.

[0006] In practice, a limitation is imposed by the lack of recognizable surficial surgical features on intra-oral objects. This limitation is often encountered in situations in which a surface is to be sampled three dimensionally for 3D modeling. There are a variety of known techniques to compensate for inadequate quantitative and qualitative surface details. These techniques for improving the acquisition of surface details, include (either separately or combined): spraying the surface of the object to be imaged with powder to improve optical properties for imaging; and projecting and/or diffracting structured illumination patterns and observing their deformation.

[0007] Several methods have been disclosed for producing maps or three-dimensional distribution models of surficial features. For example, active triangulation is a specific method that uses an active light spot and several cameras for measuring the distribution of objects on a surface. Scanning the active light spot can produce a whole map of a surface. Photogrammetry is a discipline in which analytic methods are applied for extracting three-dimensional information from photographs. Photogrammetry, as well as any discipline based on images, extends easily to map production because of the range of information obtained by the cameras employed.

[0008] As suggested above, it is well-known that making three-dimensional measurements of an intra-oral scene for the purpose of electronically constructing a model of the distribution of features, can be achieved by obtaining multi-view images of the intra-oral scene and subsequently applying appropriate analytical algorithms to the images. At least two images of the same intra-oral scene are acquired from different viewing angles. Matching features in the intra-oral scene are searched in the corresponding images. To calculate the relative height (z-dimension) of a feature, the parallax between matching appearances of the feature in different images of the same intra-oral scene is calculated via triangulation, from which the distance of the feature from a reference point is computed. Several common techniques for increasing the distinctness of the features in the images are discussed below.

[0009] Figure 1, to which reference is now made, is a flow-chart describing the order of steps that takes place in the course of a common prior-art three-dimensional modeling of a site of interest. In a step 40 the distinctiveness of features in the intra-oral scene is enhanced. In a step 42 images are acquired of the site of interest at different angles. In a step 44 matching is accomplished between features at the different images acquired. In a step 46 the parallax is measured for identical features in different images. In a step 48 the values on the z-axis are calculated for the identified features. A 3D map, or model, can then be compiled, describing the distribution of the identified features in the xyz-space.

[0010] As previously noted, however, a significant limitation in dental work is the lack of surface detail in many situations. Without a substantial amount of surface detail, it is not possible to unambiguously match surface features for accurate triangulation. To solve this problem, instead of illuminating the intra-oral scene uniformly and trying to match features through complex pattern-recognition algorithms, a well-known method is to scan a beam of light across the intra-oral scene to create an array of highlighted lines or points. This "structured illumination" can then be used for matching features in the triangulation previously mentioned. The resulting 3D model is a "wire mesh" or "polyhedral" model of the intra-oral scene. This is an advantageous approach, because the resolution of the model can be easily varied by changing the density of the scanned lines or points over the intra-oral scene, and for many intra-oral scenes of interest, the regions between the lines or points (which are not illuminated by the structured illumination) can be approximated through various smoothing functions. The result is a model of adjustable accuracy which can be analyzed using relatively simple algorithms.

[0011] Unfortunately, however, scanning (which is essentially a one-dimensional, or "1D" approach) can sometimes require excessive time, particularly if high resolution is desired. In contrast, imaging (which is a two-dimensional, or "2D" approach) can capture a much greater amount of information in the same time - or, alternatively, can capture the same amount of information in a much smaller time. This factor is important when considering the above-mentioned time limitation, in order to reduce the detrimental effects of patient, practitioner, and apparatus movement.

[0012] U.S. Patent number 4,687,325 to Corby (herein denoted as "Corby") notes that it is also possible to employ structured illumination using a single image of the intra-oral scene, whereby the triangulation is performed relative to a stored image (or the data corresponding thereto) of the structured illumination as projected on a plane or other surface of known curvature. Corby, however, is limited to the use of a one-dimensional scanning methodology, which (as discussed above) may not be suitable for certain dental applications because of the patient / practitioner movement that is likely to be encountered. Hans-Gerd Maas in International Archives of Photogrammetry and Remote Sensing Vol. XXIX part B5, pages 709 - 713 (1992), the contents of which article are incorporated by reference for all purposes as if set forth fully herein, likewise teaches the use of a perfect grid projected on a close object whose surface is to be computed. The projected grid deviates from its original form at the surface from which it reflects, and those deviations from the perfect grid are used to compile the three-dimensional model for the reflective surface. A limitation associated with the employment of regular grids is that of discontinuities and ambiguities. In the case of a discontinuity, a broken grid appearing over the reflecting surface is caused by the discontinuous relief. Broken grid lines are a cause for errors because of the ambiguities introduced by this phenomenon.

[0013] Other prior art includes U.S. patent 4,952,149 to Duret et al. (herein denoted as "Duret"), wherein a method and apparatus is disclosed for taking impressions of a portion of the body which utilizes the projection of a grid of sinusoidal profile onto the body portion of which the impression is to be taken. In U.S. patent 4,964,770 to Steinbichler et al. (herein denoted as "Steinbichler"), a process is disclosed for making artificial teeth, where horizontal or other contour lines are generated on the ground tooth stump and on adjacent surfaces to create a three-dimensional map. Three-dimensional reconstruction is achieved by the use of interferometry, moiré, and laser scanning methods. In U.S. patent 5,372,502 to Massen et al. (herein denoted as "Massen 502"), an invention is based on calculating a topographic representation by comparing between a digital image of known pixel detail projected onto a tooth surface and the resulting distorted image reflected off the tooth surface, in accordance with moiré, phase-shift, triangulation, and photogrammetry techniques. Through a comparison between the undistorted pattern projected by the probe and the distorted pattern reflected from the specific area within the oral cavity, topographical information of the imaged teeth is obtained. In U.S. patent 5,386,292 to Massen et al. (herein denoted as "Massen '292"), an invention is

described of an error factor that corrects image distortions due to factors such as enamel translucency. In U.S. patent 6,529,627 to Callari, et al., by a system is described that uses structured illumination that is manually projected on an object and by deriving the 3D model by integrating the 3D data into the initial 3D model.

[0014] One of the recognized problems in using structured light in lines or points is that of *aliasing*, or false matching of the structured illumination. A plain point of light is normally indistinguishable from other plain points of light, and so there can arise ambiguities in matching the same point from one image to another. If two different points are mistakenly matched when triangulating different images, the resulting z-axis calculation will be in error, and the 3D model will be defective. (The same problem applies to the use of lines.) In real-time scanning using electronic imaging, synchronizing the output from the different image sensors serves as an anti-aliasing mechanism. However, this cannot be employed for projected (non-scanned) images or for stored images where features are matched after the structured illumination has been projected, because there is no timing information. It also cannot be used with the single imaging method mentioned above. Several anti-aliasing methods, using different schemes of encoding the structured illumination, are described in Corby. Some of these methods involve modulating the structured illumination in wavelength and/or intensity. Corby's own method involves encoding spatially-modulated predetermined patterns in the scanned light, which can be unambiguously matched in the different images.

[0015] Once again, the time limitation presented above is noted for dental applications. In particular, certain prior art schemes would require illuminating the same areas of the intra-oral scene with patterns over a prolonged time period or repeatedly at different times. These practices, however, can introduce inaccuracies in the measurements due to any relative movement between the dental patient, the apparatus that projects the illumination, and the apparatus that captures the images (camera). This condition is exacerbated if the apparatus is being held or manipulated by the dental practitioner, because in this case there is an additional source of movement involved.

[0016] U.S. Patent number 6,167,151 to Albeck, et al. (herein denoted as "Albeck '151") discloses a means of creating a spatially-modulated random pattern by the phenomenon of laser speckle, which can then be used in a similar manner to the predetermined patterns of Corby, for identifying corresponding points in multiple images. An advantage of random patterns over predetermined patterns in anti-aliasing is that certain random systems can mathematically generate a large number of distinct patterns easily, whereas systems of distinct predetermined patterns are generally more restricted and thus limited in number. On the other hand, however, predetermined patterns (such as in Corby) can be set up in advance to be absolutely distinguishable. Random patterns, in contrast, are not predetermined, and therefore may exhibit some similarities among themselves. The patterns of Albeck '151, for example, which depend on the interference properties of coherent light upon uneven surfaces, are probabilistic and therefore different patterns can be similar in appearance, even though this is unlikely. The anti-aliasing of Albeck '151, therefore, is statistical rather than absolute.

[0017] A principal limitation of Albeck '151 is that the random patterns, being created by a physical process (laser speckle), can be neither stored nor reproduced. This requires that the multiple images of the intra-oral scene under the structured illumination be captured simultaneously in order that the same random speckle patterns be included in the different images. The fact that the random patterns of Albeck '151 cannot be stored or reproduced also precludes using a single image of the intra-oral scene under the structured illumination which is later referenced to a previously-stored image of the structured illumination impinging on a known surface, such as a planar surface (previously noted to have been described in Corby).

[0018] US 2003/0096210 A1 discloses a scanner which acquires images of the dentition which are converted to three-dimensional frames of data using a decoding process.

[0019] As noted above, an important limitation is imposed by the small space inside the mouth, which does not permit the introduction of bulky apparatus. In particular, it would be highly advantageous to use only a single imaging sensor (producing a single image or single projection) to capture the structured illumination patterns on the intraoral features for comparison with the recorded structured illumination patterns on a known surface. Doing so would significantly reduce the amount of apparatus placed in the mouth and be responsive to the space limitation of dental applications, as previously noted. Furthermore, it would be desirable to employ an imaging, rather than a scanning technique, to eliminate problems caused by movement of the patient and/or the practitioner.

[0020] WO2004017020A1 discloses measuring the relief variations of an object and/or to the deformations of said object in the direction of the relief thereof (z). A measuring device comprises an inclined optical projection means for displaying the reference image of a rough plastering whose grains are pseudo-randomly distributed, and visualisation means for obtaining the test image of the thus illuminated object. The position variations of the grains of the rough plastering between the test image and the reference image which represent the variations in the relief of the object are measured by correlation with the aid of comparison

means.

[0021] US2003096210 (A1) discloses interactive, computer based orthodontist treatment planning, appliance design and appliance manufacturing. A scanner acquires images of the dentition which are converted to three-dimensional frames of data. The data from the several frames are registered to each other to provide a complete three-dimensional virtual model of the dentition.

[0022] US4663720 discloses a method of making a dental prosthesis in which data representing standard tooth shapes and sizes, relationships between teeth and adjacent and occlusive teeth and characteristics for securing a prosthesis to a prepared site, and machining instructions for shaping a blank to the configuration of a dental prosthesis for direct implantation are stored in a computer memory.

[0023] WO2007080563A2 discloses a process for detecting the spatial structure of a three-dimensional surface by projection of a pattern on to the surface along a projection direction which defines a first axis, and by pixel-wise detection of at least one region of the pattern projected on to the surface, by means of one or more sensors in a viewing direction of the sensor or sensors, which defines a second axis, wherein the first and the second axes (or a straight line parallel to the second axis) intersect at an angle different from 0 DEG so that the first and the second axes (or the straight line parallel thereto) define a triangulation plane, wherein the pattern is defined at least upon projection into a plane perpendicularly to the first oral scene and appears in the captured image. The "z" information in the intra-oral scene is then recovered from the camera image of the scene under the structured illumination by performing a triangulation of each of the patterns in the array on the single image with reference to an image of the structured illumination projected on a reference plane, which was also illuminated from the first angle.

[0024] In order to unambiguously match corresponding points in the image of the intra-oral scene and in the stored image, the points of the structured illumination are spatially-modulated with two-dimensional random patterns which have been generated and saved in a projectable medium, a non-limiting example of which is a photographic slide. Unlike the prior-art random patterns of Albeck '151, the random patterns of the present invention are reproducible, so that the patterns projected onto the intra-oral scene to be imaged are the same as the corresponding patterns in the saved image. Furthermore, unlike the prior-art patterns of Corby, which are one-dimensional, the patterns of certain preferred embodiments of the present invention are two-dimensional.

[0025] Therefore, there is provided a method for three-dimensional modeling of the surface features of an intraoral scene for a dental application according to claim 1 and a system for three-dimensional modeling of the surface features of an intraoral scene for a dental application according to claim 4.

BRIEF DESCRIPTION OF THE DRAWINGS

[0026] The invention is herein described, by way of example only, with reference to the accompanying drawings, wherein:

Figure 1 is a flow-chart of a prior art method for three dimensional modeling of an intra-oral scene using multi-view imagery.

Figure 2A illustrates examples of random patterns for structured illumination according to embodiments of the present invention.

Figure 2B illustrates the examples of Figure 2A as detected patterns according to embodiments of the present invention.

Figure 3 illustrates examples of one-dimensional random patterns for structured illumination according to an embodiment of the present invention.

Figure 4 is a flow-chart of a method for generating and storing structured illumination patterns and producing three-dimensional models of intra-oral scenes according to an embodiment of the present invention.

Figure 5 is a block diagram illustrating a system according to an embodiment of the present invention.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0027] The principles and operation of a method according to the present invention may be understood with reference to the drawings and the accompanying description.

[0028] In accordance with the present invention, structured illumination containing stored random patterns is used to convey surficial features to an intra-oral scene to be modeled in three dimensions by a single image, wherein triangulation is performed relative to a stored image of the structured illumination impinging from a different angle on a known surface, such as a plane. The method of the invention can be applied in various dental applications and fields, as well as be put to use in dental veterinary practice, and forensic dental medicine. In a preferred embodiment of the present invention, the light projected on the site of interest within the mouth bears randomly-structured and randomly-distributed patterns such that each projected pattern is probabilistically unique over the entire area onto which the light has been projected. To illustrate the method of the invention reference is made to Figure 2A and Figure 2B. An acquired image **60** is bounded by boundary line **62**. Within image **60**, several distinct pixel aggregates **64**, **66**, and **68** are apparent, such that each aggregate forms a distinct pattern which is different from the other patterns, and also being distinctly different from a background **70**. In Figure 2B, a pattern **84** is now defined as a separate entity, delineated schematically by a dashed line ellipsoid. A pattern **86** is likewise defined and delineated, and a pattern **88** is a third pattern so delineated. It is once again noted that these patterns of the present invention are two-dimensional, in contrast to prior-art patterns, such as those of Corby, which are one-dimensional.

[0029] In accordance with the present invention, the saved random patterns are projected on the intra-oral scene to be modeled, such that the probability for a certain pattern to appear more than once on the projected area is extremely low. At the image level, a projected pattern is defined as a specific pattern of aggregated pixels. An additional aspect of certain embodiments of the present invention is that any pixel pattern is characterized not only by its form, i.e. the specific shapes formed by the pixels at each point, but also by the distribution (i.e., the order and relative proximity to other patterns) of the patterns within the structured illumination. Hence, the order and relative proximity to other patterns within the image can be used to distinguish points from one another and to properly match corresponding points in the different images. In particular, in certain embodiments of the present invention the patterns are randomly distributed over an intra-oral scene, in addition to being randomly shaped. The term "randomly distributed" herein denotes that a pattern itself, separate from the shape thereof, has been generated with a random position in the intra-oral scene.

[0030] Thus in Figure 2B, at the image level, pattern **84** (which is equivalent to pattern **64**) lies to the left of pattern **86** (which is equivalent to pattern **66**) and pattern **88** (which is equivalent to pattern **68**) in a clockwise order. As can be seen, the identified patterns not only differ from each other, but also are distributed and have a spatial relationship with other patterns of the image.

[0031] When matching patterns corresponding to the same single point of the structured illumination are obtained in the image of the intra-oral scene and the reference image, triangulation can be performed to determine the z-axis position of the pattern. The x-y positions of the pattern can be obtained directly from the image. Together, the three-dimensional x-y-z position of the pattern can thus be obtained for 3D modeling.

One-Dimensional Random Patterns

[0032] Figure 3 illustrates an example of a randomly-generated pattern **101** whose random information content extends one-dimensionally in a direction **103** in the x-y plane. The pattern contains bands of varying width, similar to the familiar "bar code" patterns, except that the widths and spacing between the bands are assigned randomly. No random information is encoded perpendicular to direction **103**. A narrow version of pattern **101** is shown in a pattern **105**.

[0033] Although the restriction of encoding the random information in a single direction limits the amount of information that can be contained in the pattern, and thereby allows a higher probability of aliasing, this can be overcome by generating a continuous pattern, which permits continuous and uninterrupted tracking across the images. That is, this form of structured illumination is conducive to the projecting of a series of scanned lines over the intra-oral scene, rather than a grid of points. The information content in the lines can therefore be increased to achieve effective anti-aliasing.

[0034] In addition, there are certain advantages to restricting the information to a single direction in a manner as presented in Figure 3. Because the information content is constrained to a direction parallel to the scan, the analysis and matching of corresponding patterns in the different images is simpler than for patterns of spots (such as illustrated in Figures 2A and 2B), where the information is two-dimensional. Thus, analysis is faster for the one-dimensional patterns as exemplified in Figure 3.

[0035] Figure 4 is a flow-chart of a method according to an embodiment of the present invention, by which random patterns are generated and saved. In a step 121 two-dimensional random patterns are generated (as previously detailed) and are saved for use in structured illumination in a two-dimensional array **123**. Array **123** may be saved utilizing photographic storage, such as in a

slide which is suitable for projecting the array onto a surface.

[0036] Then, array **123** with the previously-described random patterns is projected onto a reference surface in a step **125** from a first angle relative to the reference surface. In an embodiment of the present invention, the reference surface is a plane. In another embodiment of the present invention, the reference surface is a general surface with a mathematical description

[0037] An image of the structured illumination on the reference surface from the projection of array **123** is acquired and saved as a reference image **127**.

[0038] Next, array **123** is projected at the previously-used first angle (see above) onto the intra-oral scene in a step **129**. In a step **131**, an image **133** of the intra-oral scene is captured from a second angle relative to the intra-oral scene. It is noted that image **133** contains the point locations where the projection of array **123** impinges on the surface of the intra-oral scene - that is, image **133** contains a two-dimensional image of the structured illumination on the surface of the intra-oral scene. Finally, in a step **135** the points of structured illumination of array **123** in image **133** are matched with the points of structured illumination of array **123** in reference image **127**, and the z-axis positions of those points are computed by triangulation, using parallax measurements, to obtain a three-dimensional model **137** of the intra-oral scene.

[0039] Figure 5 is a schematic representation of a system for three-dimensional modeling of the surface features of an intra-oral scene for a dental application, the system comprising a generator **51** for generating a two-dimensional array of a plurality of random, one or two-dimensional patterns. The pattern created is stored in a storage medium operative to allow projecting said array **52**, and a first projector **92** for projecting said array from said projectable medium onto a reference surface **93** from a first angle. An acquisition unit **94** is a first acquiring means for acquiring a first image **95** of said array projected on said reference surface from a second angle. A second projector **92** is used for projecting said array from said projectable medium onto the intra-oral scene at said first angle and a second acquiring means, and acquisition unit **53** for acquiring a second image **55** of said array projected on the intra-oral scene from said second angle. A first position calculator **56** is used for calculating the two-dimensional relative positions of said random patterns based on the relative positions thereof in an image, and a pattern-matching means for matching said random two-dimensional patterns in said first image **95** with said random two-dimensional patterns in said second image **55**. A parallax calculator **57** is used for calculating the parallax between said random patterns in said first image **95** with said random patterns in said second image **96**. A second position calculator **58** is used for calculating three-dimensional relative positions of the random patterns based on the two-dimensional relative positions and said parallax, and a modeling means **59** for constructing a three-dimensional model of the intra-oral scene based on said three-dimensional relative positions. A system used by the user needs the reference image but not the means of generating the reference image.

Multiple Imaging

[0040] Although the use of a single image is preferable in intra-oral use because of space constraints, it is also possible to use the present invention with multiple images as well. In this case, embodiments of the present invention utilize the above method for generating storable random structured illumination patterns as described herein, and then using those patterns with multiple-imaging techniques as exemplified in Figure 1 and previously described.

Uses of the Invention

[0041] In dentistry, reconstitution of dental elements is a common practice. Projecting illuminated structures on intra oral objects to be modeled, can provide for an inexpensive yet advantageous background for a potentially efficacious 3D modeling of the oral cavity parts. Other applications for 3D mapping of intra-oral features include, but are not limited to: forensic dental medicine; insurance purposes; examination and treatment planning; and treatment automation. This particular invention is advantageous as it does not require a perfect projection on an ideal surface, and existing surficial features present on intra oral objects may even enhance the random surficial pattern.

[0042] While the invention has been described with respect to a limited number of embodiments, it will be appreciated that many variations, modifications and other applications of the invention may be made.

REFERENCES CITED IN THE DESCRIPTION

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PATENTKRAV

1. Fremgangsmåde til tredimensionel modellering af overfladeegenskaberne for en intraoral scene til en dental anvendelse, hvilken fremgangsmåde omfatter:

- 5 • generering af en todimensionel fremstilling af en flerhed af todimensionelle mønstre, der er vilkårlige i én retning, eller generering af en todimensionel fremstilling af en flerhed af todimensionelle mønstre, der er vilkårlige i to retninger, hvor hvert af flerheden af todimensionelle mønstre indbefatter pixelaggregater og hvert af pixelaggregaterne danner et særskilt mønster, der adskiller sig fra de andre mønstre af flerheden af todimensionelle mønstre og også
10 adskiller sig væsentligt fra en baggrund;
- lagring af fremstillingen i et projicerbart medium;
- projicering af fremstillingen fra det projicerbare medium på en referenceoverflade fra en første vinkel;
- opnåelse af et første billede af fremstillingen projiceret på referenceoverfladen,
15 hvor opnåelse af det første billede udføres fra en anden vinkel;
- projicering af fremstillingen fra det projicerbare medium på den intraorale scene fra den første vinkel;
- opnåelse af et andet billede af fremstillingen projiceret på den intraorale scene fra den anden vinkel;
- 20 • opnåelse af x-y-information i den intraorale scene fra det andet billede;
- opnåelse af z-information i den intraorale scene ved udførelse af en triangulering af hvert af mønstrene i fremstillingen på det andet billede med reference til det første billede og
- konstruktion af en tredimensionel model af den intraorale scene baseret på x-y-
25 og z-informationen.

2. Fremgangsmåde ifølge krav 1, hvor den intraorale scene indeholder mindst en del af et intraoralt objekt.

30 3. Fremgangsmåde ifølge krav 1, hvor de todimensionelle mønstre er vilkårligt fordelt i fremstillingen.

4. System til tredimensionel modellering af overfladeegenskaberne for en intraoral scene til en dental anvendelse, hvilket system omfatter:

- en todimensionel fremstilling af en flerhed af todimensionelle mønstre, der er vilkårlige i én retning, eller en todimensionel fremstilling af en flerhed af todimensionelle mønstre, der er vilkårlige i to retninger, hvor hvert af flerheden af todimensionelle mønstre indbefatter pixelaggregater og hvert af pixelaggregaterne danner et særskilt mønster, der adskiller sig fra de andre mønstre af flerheden af todimensionelle mønstre og også adskiller sig væsentligt fra en baggrund;
 - et lagringsmedium til fremstillingen, hvilket lagringsmedium kan anvendes til at tillade projicering af fremstillingen;
 - et opnåelsesmiddel til opnåelse af et første billede af fremstillingen projiceret på en referenceoverflade
 - en projektor til projicering af fremstillingen fra lagringsmediet på den intraorale scene i en første vinkel;
 - et opnåelsesmiddel til opnåelse af et andet billede af fremstillingen projiceret på den intraorale scene fra en anden vinkel;
 - en første positionsberegner til beregning af de todimensionelle relative positioner af de vilkårlige mønstre baseret på de relative positioner deraf i et billede;
 - et opnåelsesmiddel til opnåelse af x-y-information i den intraorale scene fra det andet billede; og
- et opnåelsesmiddel til opnåelse af z-information i den intraorale scene ved udførelse af en triangulering af hvert af mønstrene i fremstillingen på det andet billede med reference til det første billede og
- et modelleringsmiddel til konstruktion af en tredimensionel model af den intraorale scene baseret på x-y- og z-informationen.

DRAWINGS

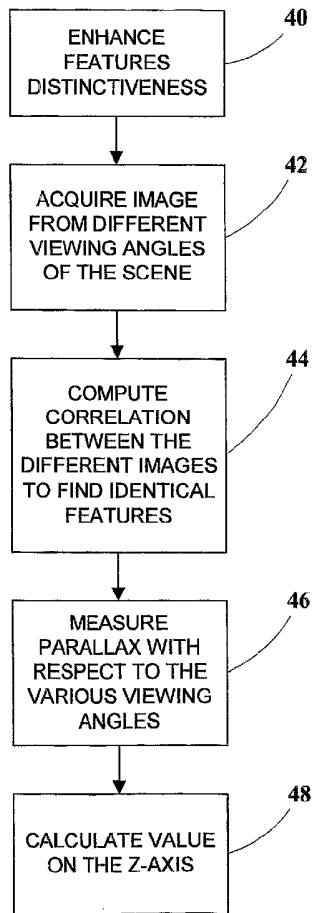


FIG. 1 (PRIOR ART)

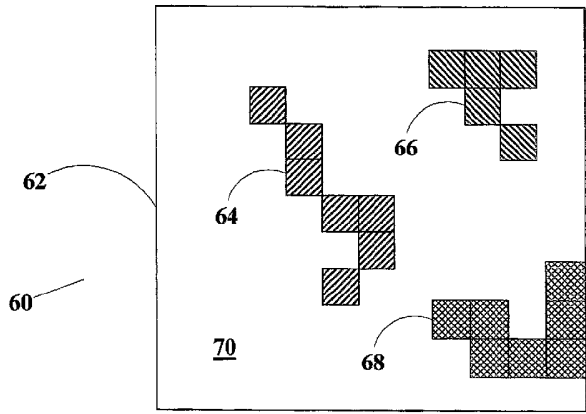


FIG. 2A

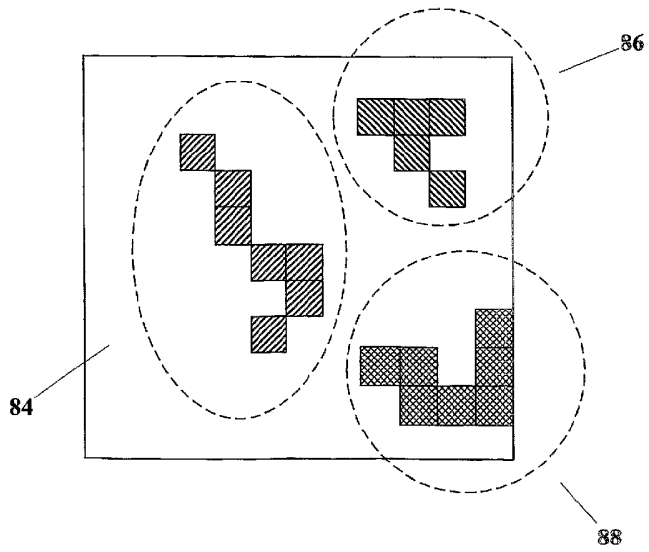


FIG. 2B

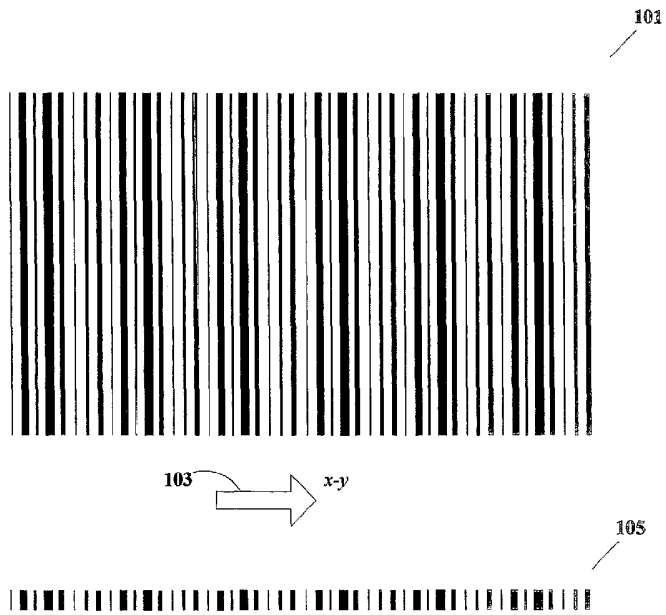


FIG.3

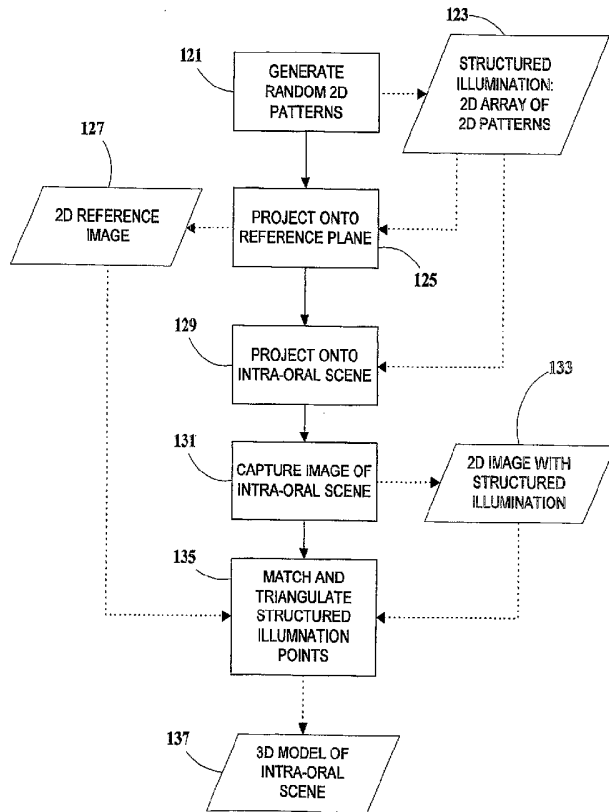


FIG. 4

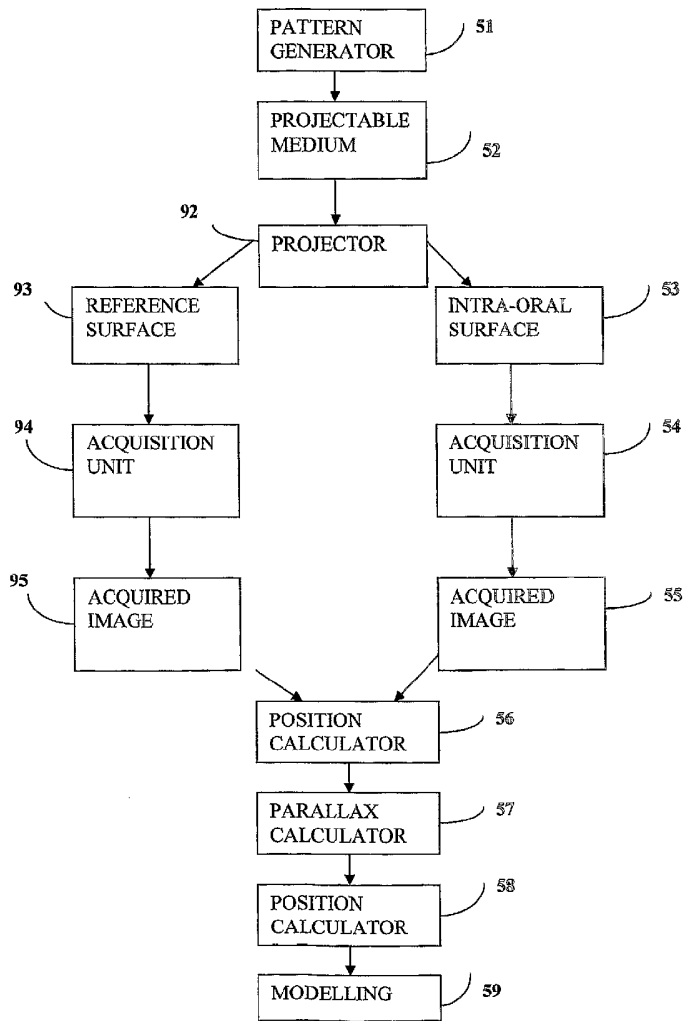


FIG. 5