



(22) Date de dépôt/Filing Date: 2003/12/12

(41) Mise à la disp. pub./Open to Public Insp.: 2004/06/18

(45) Date de délivrance/Issue Date: 2012/02/07

(30) Priorité/Priority: 2002/12/18 (US10/322,154)

(51) Cl.Int./Int.Cl. *C08F 220/08* (2006.01),  
*A61L 17/00* (2006.01), *A61L 17/14* (2006.01),  
*A61L 24/04* (2006.01), *A61L 27/34* (2006.01),  
*A61L 31/10* (2006.01), *C08F 216/02* (2006.01),  
*C08F 216/04* (2006.01), *C08F 220/04* (2006.01),  
*C08G 63/52* (2006.01), *C08G 63/91* (2006.01),  
*C08J 5/00* (2006.01), *C08L 29/02* (2006.01),  
*C08L 33/00* (2006.01), *C08L 33/02* (2006.01)

(72) Inventeur/Inventor:  
NATHAN, ARUNA, US

(73) Propriétaire/Owner:  
ETHICON, INC., US

(74) Agent: NORTON ROSE CANADA  
S.E.N.C.R.L., S.R.L./LLP

(54) Titre : POLYMERES COMPORTANT DES GROUPEMENTS FONCTIONNELS POUR DES APPLICATIONS  
MEDICALES

(54) Title: FUNCTIONALIZED POLYMERS FOR MEDICAL APPLICATIONS

(57) **Abrégé/Abstract:**

The present invention is directed to synthetic, biodegradable, biocompatible polymers that are the reaction product of an  $\alpha,\beta$ -unsaturated polybasic acid or derivative thereof and a monoglyceride, and which further contain pended thereto a functional agent, and to medical devices and compositions containing such polymers.

**ABSTRACT OF THE INVENTION**

5           The present invention is directed to synthetic,  
biodegradable, biocompatible polymers that are the  
reaction product of an  $\alpha,\beta$ -unsaturated polybasic acid or  
derivative thereof and a monoglyceride, and which  
further contain pended thereto a functional agent, and  
to medical devices and compositions containing such  
10           polymers.

**FUNCTIONALIZED POLYMERS FOR MEDICAL APPLICATIONS**

5

**FIELD OF THE INVENTION**

The present invention relates to synthetic, biodegradable, biocompatible polymers for use in pharmaceutical and medical applications and to compositions and medical devices containing such polymers.

10

**BACKGROUND OF THE INVENTION**

15

Both natural and synthetic polymers, including homopolymers and copolymers, which are both biocompatible and biodegradable *in vivo* are known for use in the manufacture of medical devices that are implanted in body tissue and that are absorbed or passed by the body over time. Examples of such medical devices include suture anchor devices, sutures, staples, surgical tacks, clips, plates, screws, drug-delivery devices, adhesion prevention films and foams, and tissue adhesives.

20

25

Natural polymers may include catgut, cellulose derivatives and collagen. Natural polymers typically are absorbed by the body after enzymatic degradation of the polymers in the body.

30

Synthetic polymers may include aliphatic polyesters, polyanhydrides and poly(orthoester)s. Such polymers typically degrade by a hydrolytic mechanism in

the body and then are absorbed by the body. Such synthetic polymers include homopolymers, such as poly(glycolide), poly(lactide), poly( $\epsilon$ -caprolactone), poly(trimethylene carbonate) and poly(p-dioxanone), and copolymers, such as poly(lactide-co-glycolide), poly( $\epsilon$ -caprolactone-co-glycolide), poly(glycolide-co-trimethylene carbonate), poly(alkylene diglycolate), and polyoxaesters. The polymers may be statistically random copolymers, segmented copolymers, block copolymers or graft copolymers.

Alkyd-type polyesters prepared by the polycondensation of a polyol, polyacid and fatty acid are used in the coating industry in a variety of products, including chemical resins, enamels, varnishes and paints. These polyesters also are used in the food industry to make texturized oils and emulsions for use as fat substitutes.

While much progress has been made in the field of polymeric biomaterials, further developments must be made in order for such biomaterials to be used optimally in the body. There is a great need for polymers for use in drug delivery, tissue engineering and medical devices, where the polymers have functional pendant groups that would allow, e.g., attachment of drugs, improvement of biocompatibility or promotion of bioadhesion. Polyesters containing functional comonomers are known. However, the chemistry involved in the synthesis of functional monomers is often very complex

and results in poor yields.

#### SUMMARY OF THE INVENTION

5 The present invention is directed to a synthetic, biodegradable, biocompatible polymer comprising the reaction product of an  $\alpha, \beta$ -unsaturated polybasic acid or derivative thereof, a monoglyceride, and further comprising a functional agent pended thereto to provide the polymer with certain desired properties. The  
10 invention also is directed to compositions for medical applications and medical devices containing such polymers.

#### DETAILED DESCRIPTION OF THE INVENTION

15 Alkyd polymers have been prepared by several known methods. For example, alkyd-type polymers were prepared by Van Bemmelen (*J. Prakt. Chem.*, 69 (1856) 84) by condensing succinic anhydride with glycerol. In the "Fatty Acid" method (see Parkyn, et al. *Polyesters*  
20 (1967), Iliffe Books, London, Vol. 2 and Patton, In: *Alkyd Resins Technology*, Wiley-Interscience New York (1962)), a fatty acid, a polyol and an anhydride are mixed together and allowed to react. The "Fatty Acid-Monoglyceride" method includes a first step of  
25 esterifying the fatty acid with glycerol and, when the first reaction is complete, adding an acid anhydride. The reaction mixture then is heated and the polymerization reaction takes place. In the "Oil-

Monoglyceride" method, an oil is reacted with glycerol to form a mixture of mono-, di-, and triglycerides. This mixture then is polymerized by reacting with an acid anhydride.

5           The synthetic, biodegradable, biocompatible polymers utilized in the present invention are the reaction product of an  $\alpha,\beta$ -unsaturated polybasic acid or derivative thereof, a monoglyceride, and a functional agent. Preferably, the polymers of the present  
10 invention are prepared by the polycondensation first of an  $\alpha,\beta$ -unsaturated polybasic acid or derivative thereof with a monoglyceride to form an alkyd polyester polymer. The monoglyceride comprises reactive hydroxy groups and fatty acid groups.

15           The alkyd polyester polymer is reacted with the functional agent to form the functionalized alkyd polyester of the present invention. The functional agent comprises a first functional moiety that is a strong nucleophile, such as a thiol or amine, that can react  
20 with the  $\alpha,\beta$ -unsaturated acid through a Michael addition reaction, thus pending the functional agent to the polymer. A "strong nucleophile" is a molecule that is capable of donating an electron pair to an electrophile in a polar-bond forming reaction. Preferably, the  
25 strong nucleophile is more nucleophilic than H<sub>2</sub>O at physiologic pH.

The functional agent also comprises a second functional moiety, such as a hydroxyl, carboxyl, amine

and the like, in order to provide the polymer with certain desired properties. For example, the functional agent may be selected to provide desired solubility properties or to adjust pH, depending upon the particular application. The functional agent may be selected based upon the ability of the second moiety's ability to react with certain therapeutic agents, e.g. pharmaceutical drugs. The second moiety also may provide desired hydrophobicity/hydrophilicity to the polymer. In addition, the adhesiveness of the polymer may be adjusted depending upon selection of the functional moiety.

The polymers comprise an aliphatic polyester backbone with pendant fatty acid ester groups on the monoglyceride unit and the second functional moiety, e.g. hydroxyl, carboxyl or amine, pendant from the diacid unit. Long chain saturated fatty acids result in polymers that are solids that exhibit relatively low melting points, e.g. between about 25°C and 70°C. Alternatively, use of unsaturated fatty acids or short chain fatty acids results in liquid polymers. As used herein, a liquid polymer is a polymer with a melt temperature of less than about 25°C, preferably less than about 20°C.

The solid polymers and/or liquid polymers can be used to form injectable microdispersions. The microdispersions can be formed by physically blending either liquid polymers or finely ground solid polymers

of the present invention with compatible polymers. In one embodiment, the microdispersions can be formed by physically blending liquid polymers of the present invention with finely ground solid polymers of the present invention. Upon blending, the solid polymer particle phase is dispersed through the polymeric liquid phase.

Generally, the solid polymers will have an average particle diameter of less than about 500 microns and preferably less than 50 microns. It is currently preferred to mix the finely ground solid polymer and the liquid polymer and raise the temperature of the mixture to a temperature sufficient to melt the solid polymer (melt blending), thereby providing a dispersion of a first polymeric liquid phase dispersed in a second polymeric liquid phase. Upon cooling, the first dispersed liquid polymeric phase participates to form a solid polymer phase dispersed in the second polymeric liquid phase. Melt blending is preferred because it simplifies the mixing operation involved in producing the microdispersion. It is desirable to avoid excessive heating during melt blending to avoid transesterification of the polymers.

Monoglycerides that may be used to prepare the polymers utilized in the present invention include, without limitation, monostearoyl glycerol, monopalmitoyl glycerol, monomyristoyl glycerol, monocaproyl glycerol, monodecanoyl glycerol, monolauroyl glycerol,

monolinoleoyl glycerol, monooleoyl glycerol, and combinations thereof. Preferred monoglycerides include monostearoyl glycerol, monopalmitoyl glycerol and monomyristoyl glycerol.

5            $\alpha$ , $\beta$ -unsaturated polybasic acids that can be used include multifunctional carboxylic acids, such as maleic, fumaric, citraconic itaconic- acid and the like. Polybasic acid derivatives include anhydrides, such as maleic anhydride, mixed anhydrides, esters, 10 activated esters and acid halides. The multifunctional carboxylic acids listed above are preferred.

In another embodiment, other polybasic acids such as succinic, glutaric, adipic, pimelic, suberic and sebacic acids could also be used to make copolymers with 15 the  $\alpha$ , $\beta$ -unsaturated acids listed above.

The functionalized alkyd polyesters of the present invention are made using the well known Michael addition reaction. The functional agent comprises a first functional moiety comprising a strong nucleophile, such as a thiol or amine, in order to provide reaction with 20 and binding to the alkyd polyester. The functional agent also comprises a second functional moiety such as an alcohol, amine, acid, sulfate, sulfonate and the like, in order to provide the functionalized alkyd 25 polyester with certain properties. The choice of the functional agent will depend on the particular polymer to be generated and also upon the properties required for the particular anticipated or desired use of the

functionalized polymer. One skilled in the art of medical devices and compositions, once having the benefit of this disclosure, will be able to readily ascertain the particular functional agent required for the particular properties desired under the particular circumstance. Suitable functional agents include, without limitation, mercaptoethanol, mercaptopropanol, mercaptobutanol, mercaptohexanol, mercaptopropanediol, mercaptoacetic acid, mercaptopropionic acid, mercaptosuccinic acid and mercaptoethylamine.

In certain embodiments of the invention, the alkyd polyester may be prepared from the polybasic acid or derivative thereof, the monoglyceride and, additionally, at least one additional polyol selected from the group consisting of ethylene glycol, 1,2-propylene glycol, 1,3-propanediol, bis-2-hydroxyethyl ether, 1,4-butanediol, 1,5-pentanediol, 1,6-hexanediol, 1,8-octanediol, 1,10-decanediol, 1,12-dodecanediol, other diols, linear poly(ethylene glycol), branched poly(ethylene glycol), linear poly(propylene glycol), branched poly(propylene glycol), linear poly(ethylene-co-propylene glycol)s and branched poly(ethylene-co-propylene glycol)s. In preparing the polymers of the present invention, the particular chemical and mechanical properties required of the polymer for a particular use must be considered. For example, changing the chemical composition can vary the physical and mechanical properties, including absorption times.

Copolymers can be prepared by using mixtures of diacids, different monoalkanoyl glycerides and different functional moieties to match a desired set of properties. Similarly, blends of two or more functionalized alkyds may be prepared to tailor properties for different applications.

A variety of biological active substances, hereinafter referred to as bioactive agents, can be covalently attached to the functionalized polymers by known coupling chemistry to provide sustained release of the bioactive agent. As used herein, bioactive agent is meant to include those substances or materials that have a therapeutic effect on mammals, e.g. pharmaceutical compounds.

The polymerization of the alkyd polyesters preferably is performed under melt polycondensation conditions in the presence of an organometallic catalyst at elevated temperatures. The organometallic catalyst preferably is a tin-based catalyst, e.g. stannous octoate. The catalyst preferably will be present in the mixture at a mole ratio of polyol and polycarboxylic acid to catalyst in the range of from about 15,000/1 to 80,000/1. The reaction preferably is performed at a temperature no less than about 120°C. Higher polymerization temperatures may lead to further increases in the molecular weight of the copolymer, which may be desirable for numerous applications. The exact reaction conditions chosen will depend on numerous

factors, including the properties of the polymer desired, the viscosity of the reaction mixture, and melting temperature of the polymer. The preferred reaction conditions of temperature, time and pressure can be readily determined by assessing these and other factors.

Generally, the reaction mixture will be maintained at about 180°C. The polymerization reaction can be allowed to proceed at this temperature until the desired molecular weight and percent conversion is achieved for the copolymer, which typically will take from about 15 minutes to 24 hours. Increasing the reaction temperature generally decreases the reaction time needed to achieve a particular molecular weight.

In another embodiment, copolymers of alkyd polyesters can be prepared by forming an alkyd polyester prepolymer polymerized under melt polycondensation conditions, then adding at least one lactone monomer or lactone prepolymer. The mixture then would be subjected to the desired conditions of temperature and time to copolymerize the prepolymer with the lactone monomers.

The molecular weight of the prepolymer, as well as its composition, can be varied depending on the desired characteristic that the prepolymer is to impart to the copolymer. Those skilled in the art will recognize that the alkyd polyester prepolymers described herein can also be made from mixtures of more than one monoglyceride and dicarboxylic acid.

The addition of the functional agent comprising the nucleophilic reagent to the alkyd polyester having an  $\alpha, \beta$ -unsaturated group can be carried out at room temperature or at 60°C for 24 hours using benzoyl peroxide/dimethylaminopyridine or azobis isobutyronitrile (AIBN) as catalyst. Alternatively, the reaction may be performed at room temperature for 14 hours using triethylamine as catalyst.

The polymers, copolymers and blends of the present invention can be crosslinked to affect mechanical properties. Crosslinking can be accomplished by the addition of crosslinking enhancers, irradiation, e.g. gamma-irradiation, or a combination of both. In particular, crosslinking can be used to control the amount of swelling that the materials of this invention experience in water.

One of the beneficial properties of the functionalized alkyd polyesters of this invention is that the ester linkages in the alkyd block are hydrolytically unstable and, therefore, the polymer is biodegradable because it readily breaks down into small segments when exposed to moist body tissue. The segments then either are absorbed by the body, or passed by the body. More particularly, the biodegraded segments do not elicit permanent chronic foreign body reaction, because they are absorbed by the body, such that no permanent trace or residual of the segment is retained by the body. In this regard, while it is envisioned that co-

reactants could be incorporated into the reaction mixture of the polybasic acid and the diol for the formation of the functionalized alkyds, it is preferable that the reaction mixture does not contain a  
5 concentration of any co-reactant that would render the subsequently prepared polymer nonbiodegradable or nonabsorbable. Preferably, the reaction mixture is substantially free of any such co-reactants if the resulting polymer is rendered nonbiodegradable or  
10 nonabsorbable.

The functionalized polymers of the present invention may be used in various medical devices for various purposes. One skilled in the art, once having the benefit of this disclosure, will be able to readily  
15 utilize the polymers in various medical devices. Examples of such medical devices include suture anchor devices, sutures, staples, surgical tacks, clips, plates, screws, drug-delivery devices, adhesion prevention films and foams, and tissue adhesives.

In one embodiment of the invention, the functionalized alkyd polyesters of the present invention can be used as a pharmaceutical carrier in a drug  
20 delivery matrix. Solid functionalized alkyd polyesters could be used to coat or encapsulate a bioactive agent. Alternatively, an effective amount of a bioactive agent  
25 could be mixed with injectable microdispersions of solid and liquid polymers. Such a microdispersion would be particularly suitable for unstable drugs such as

proteins.

The variety of bioactive agents that can be used in conjunction with the polymers of the invention is vast. In general, bioactive agents which may be administered via pharmaceutical compositions of the invention include, without limitation, antiinfectives, such as antibiotics and antiviral agents; analgesics and analgesic combinations; anorexics; antihelmintics; antiarthritics; antiasthmatic agents; anticonvulsants; antidepressants; antidiuretic agents; antidiarrheals; antihistamines; antiinflammatory agents; antimigraine preparations; antinauseants; antineoplastics; antiparkinsonism drugs; antipruritics; antipsychotics; antipyretics; antispasmodics; anticholinergics; sympathomimetics; xanthine derivatives; cardiovascular preparations including calcium channel blockers and beta-blockers such as pindolol and antiarrhythmics; antihypertensives; diuretics; vasodilators, including general coronary, peripheral and cerebral; central nervous system stimulants; cough and cold preparations, including decongestants; hormones, such as estradiol and other steroids, including corticosteroids; hypnotics; immunosuppressives; muscle relaxants; parasympatholytics; psychostimulants; sedatives; tranquilizers; naturally derived or genetically engineered proteins, growth factors, polysaccharides, glycoproteins or lipoproteins; oligonucleotides; antibodies; antigens; cholinergics; chemotherapeutics;

hemostatics; clot dissolving agents; radioactive agents; and cystostatics.

Rapamycin, risperidone, and erythropoietin are preferred bioactive agents that may be used in drug  
5 delivery matrices of the present invention.

The drug delivery matrix may be administered in any suitable dosage form such as oral, parenteral, pulmonary, buccal, nasal, ocular, topical, vaginal routes, or as a suppository. Bioerodible particles,  
10 ointments, gels, creams, and similar soft dosage forms adapted for the administration via the above routes may also be formulated. Other modes of administration, e.g. transdermal, and compositional forms, e.g. more rigid transdermal forms, are within the scope of the invention  
15 as well.

Parenteral administration of a bioerodible composition of the invention can be effected by either subcutaneous or intramuscular injection. The bioactive agent could be encapsulated in particles made of the  
20 solid polymer. Alternatively, parenteral formulations of the copolymer may be formulated by mixing one or more pharmaceuticals with a liquid copolymer or microdispersion. Other suitable parenteral additives may be formulated with the copolymer and pharmaceutical  
25 active. However, if water is to be used it should be added immediately before administration. Bioerodible ointment, gel or cream may also be injected as is or in combination with one or more suitable auxiliary

components as described below. Parenteral delivery is preferred for administration of proteinaceous drugs such as growth factors, growth hormone, or the like.

5 The bioerodible ointments, gels and creams of the invention will include an ointment, gel or cream base comprising one or more of the copolymers described herein and a selected bioactive agent. The bioactive agent, whether present as a liquid, a finely divided solid, or any other physical form, is dispersed in the  
10 ointment, gel or cream base. Typically, but optionally, the compositions include one or more other components, e.g., nontoxic auxiliary substances such as colorants, diluents, odorants, carriers, excipients, stabilizers or the like.

15 The quantity and type of copolymers incorporated into the parenteral, ointment, gel, cream, etc., is variable. For a more viscous composition, a higher molecular weight polymer is used. If a less viscous composition is desired, a lower molecular weight polymer  
20 can be employed. The product may contain blends of the liquid or low melting point copolymers to provide the desired release profile or consistency to a given formulation.

25 While not essential for topical or transdermal administration of many drugs, in some cases, it may be preferred that a skin permeation enhancer be co-administered with the drug. Any number of the many skin permeation enhancers known in the art may be used.

Examples of suitable enhancers include dimethylsulfoxide (DMSO), dimethylformamide (DMF), N, N-dimethylacetamide (DMA), deslymethyloxide, ethanol, eucalyptol, lecithin, and the 1-N-dodecylcyclazacycloheptan-2-ones.

5 Depending on dosage form, the pharmaceutical compositions of the present invention may be administered in different ways, i.e. parenterally, topically, or the like. Preferred dosage forms are liquid dosage forms that can be administered  
10 parenterally.

The amount of bioactive agent will be dependent upon the particular drug employed and medical condition being treated. Typically, the amount of drug represents about 0.001% to about 70%, more typically about 0.001%  
15 to about 50%, most typically about 0.001% to about 20% by weight of the matrix.

The quantity and type of alkyd incorporated into the parenteral will vary depending on the release profile desired and the amount of drug employed. The  
20 product may contain blends of polymers to provide the desired release profile or consistency to a given formulation.

The functionalized alkyd polyester, upon contact with body fluids, including blood or the like, undergoes  
25 gradual degradation, mainly through hydrolysis, with concomitant release of the dispersed drug for a sustained or extended period, as compared to the release from an isotonic saline solution. This can result in

prolonged delivery of effective amounts of drug, e.g. over about 1 to about 2,000 hours, preferably about 2 to about 800 hours, or, e.g. 0.0001 mg/kg/hour to 10 mg/kg/hour. This dosage form can be administered as is necessary, depending on the subject being treated, the severity of the affliction, the judgment of the prescribing physician, and the like.

Individual formulations of drugs and polyether alkyd may be tested in appropriate *in vitro* and *in vivo* models to achieve the desired drug release profiles. For example, a drug could be formulated with a functionalized alkyd polyester and orally administered to an animal. The drug release profile could then be monitored by appropriate means, such as by taking blood samples at specific times and assaying the samples for drug concentration. Following this or similar procedures, those skilled in the art will be able to formulate a variety of formulations.

In a further embodiment of the present invention, the polymers and blends thereof can be used in tissue engineering applications, e.g. as supports for cells or delivery vehicle for cells. Appropriate tissue scaffolding structures are known in the art, such as the prosthetic articular cartilage described in U.S. Pat. No. 5,306,311, the porous biodegradable scaffolding described in WO 94/25079, and the prevascularized implants described in WO 93/08850. Methods of seeding

and/or culturing cells in tissue scaffoldings are also known in the art such as those methods disclosed in EPO 422 209 B1, WO 88/03785, WO 90/12604 and WO 95/33821, all of which are all hereby incorporated by reference herein as if set forth in their entirety.

In another embodiment, the functionalized alkyd polyester is used to coat a surface of a medical device to enhance the lubricity of the coated surface. The polymer may be applied as a coating using conventional techniques. For example, the polymer may be solubilized in a dilute solution of a volatile organic solvent, such as acetone, methanol, ethyl acetate or toluene, and then the article can be immersed in the solution to coat its surface. Once the surface is coated, the surgical article can be removed from the solution where it can be dried at an elevated temperature until the solvent and any residual reactants are removed.

Although it is contemplated that numerous surgical articles, including but not limited to endoscopic instruments, can be coated with the polymers of this invention to improve the surface properties of the article, the preferred surgical articles are surgical sutures and needles. The most preferred surgical article is a suture, most preferably attached to a needle. Preferably, the suture is a synthetic absorbable suture. These sutures are derived, for example, from homopolymers and copolymers of lactone monomers such as glycolide, lactide, including L-lactide

D-lactide, meso-lactide and rac-lactide,  $\epsilon$ -caprolactone, p-dioxanone, 1,4-dioxanone, 1,4-dioxepan-2-one, 1,5-dioxepan-2-one and trimethylene carbonate. The preferred suture is a braided multifilament suture  
5 composed of polyglycolide or poly(glycolide-co-lactide).

The amount of coating polymer to be applied on the surface of a braided suture can be readily determined empirically and will depend on the particular copolymer and suture chosen. Ideally, the amount of coating  
10 copolymer applied to the surface of the suture may range from about 0.5 to about 30 percent of the weight of the coated suture, more preferably from about 1.0 to about 20 weight percent, most preferably from 1 to about 5 weight percent. If the amount of coating on the suture  
15 were greater than about 30 weight percent, then it may increase the risk that the coating may flake off when the suture is passed through tissue.

Sutures coated with the polymers of this invention are desirable because they have a more slippery feel,  
20 thus making it easier for the surgeon to slide a knot down the suture to the site of surgical trauma. In addition, the suture is more pliable and, therefore, is easier for the surgeon to manipulate during use. These advantages are exhibited in comparison to sutures which  
25 do not have their surfaces coated with the polymer of this invention.

In another embodiment of the present invention, when the article is a surgical needle, the amount of

coating applied to the surface of the article is an amount which creates a layer with a thickness ranging preferably between about 2 to about 20 microns on the needle, more preferably about 4 to about 8 microns. If the amount of coating on the needle were such that the thickness of the coating layer was greater than about 20 microns, or if the thickness was less than about 2 microns, then the desired performance of the needle as it is passed through tissue may not be achieved.

In another embodiment of the present invention, functionalized alkyd polyesters of the present invention can be used to overcoat microparticles encapsulating a bioactive agent(s). This would help provide an additional barrier for sustained release of the drug.

In yet another embodiment, the functionalized alkyd polyesters of the present invention could be used to form a bone replacement material comprising the solid polymer, or the liquid polymer, or a microdispersion of the polymers of the current invention and inorganic filler. The inorganic filler may be selected from alpha-tricalcium phosphate, beta-tricalcium phosphate, calcium carbonate, barium carbonate, calcium sulfate, barium sulfate, hydroxyapatite, and mixtures thereof. In certain embodiments the inorganic filler comprises a polymorph of calcium phosphate. Preferably, the inorganic filler is hydroxyapatite. The bone replacement materials may further comprise a bioactive agent in a therapeutically effective amount, such a

growth factor, to facilitate growth of bone tissue. Furthermore, the bone replacement material may comprise a biologically derived substance selected from the group consisting of demineralized bone, platelet rich plasma, bone marrow aspirate and bone fragments. The relative amounts of polymeric wax and inorganic filler may be determined readily by one skilled in the art by routine experimentation after having the benefit of this disclosure.

10           The injectable microdispersions can be used for a variety of soft tissue repair and augmentation procedures. For example, the microdispersions can be used in facial tissue repair or augmentation, including but not limited to camouflaging scars, filling  
15           depressions, smoothing out irregularity, correcting asymmetry in facial hemiatrophy, second branchial arch syndrome, facial lipodystrophy and camouflaging age-related wrinkles as well as augmenting facial eminences, e.g. lips, brow, etc. Additionally, these injectable  
20           microdispersions can be used to restore or improve sphincter function, such as for treating stress urinary incontinence. Other uses of these injectable  
25           microdispersions may also include the treatment of vesicoureteral reflux (incomplete function of the inlet of the ureter in children) by subureteric injection and the application of these microdispersions as general purpose fillers in the human body.

Surgical applications for an injectable, biodegradable microdispersion include, but are not limited to, facial contouring, e.g. frown or glabellar line, acne scars, cheek depressions, vertical or perioral lip lines, marionette lines or oral commissures, worry or forehead lines, crow's feet or periorbital lines, deep smile lines or nasolabial folds, smile lines, facial scars, lips and the like; periurethral injection, including injection into the submucosa of the urethra along the urethra, at or around the urethral-bladder junction to the external sphincter; urethral injection for the prevention of urinary reflux; injection into the tissues of the gastrointestinal tract for the bulking of tissue to prevent reflux; to aid in sphincter muscle coaptation, internal or external, and for coaptation of an enlarged lumen; intraocular injection for the replacement of vitreous fluid or maintenance of intraocular pressure for retinal detachment; injection into anatomical ducts to temporarily plug the outlet to prevent reflux or infection propagation; larynx rehabilitation after surgery or atrophy; and any other soft tissue which can be augmented for cosmetic or therapeutic effect. Surgical specialists who would use such a product include, but are not limited to, plastic and reconstructive surgeons; dermatologists; facial plastic surgeons, cosmetic surgeons, otolaryngologists; urologists; gynecologists; gastroenterologists;

ophthalmologists; and any other physician qualified to utilize such a product.

5           Additionally, to facilitate the administration and treatment of patients with the inventive microdispersion, pharmaceutically active compounds or adjuvants can be administered therewith. Pharmaceutically active agents that may be co-administered with the inventive microdispersion include, but are not limited to, anesthetics, e.g. lidocaine; and  
10           antiinflammatories, e.g. cortisone.

          The microdispersion can be administered with a syringe and needle or a variety of devices. It is also envisioned that the microdispersion could be sold in the form of a kit comprising a device containing the  
15           microdispersion. The device having an outlet for said microdispersion, an ejector for expelling the microdispersion and a hollow tubular member fitted to the outlet for administering the microdispersion into an animal.

20           The dosage forms for the microdispersions of the invention are sustained-release parenterals, bioerodible ointments, gels, creams, and similar soft dosage forms.

          The examples set forth below are for illustration purposes only and are not intended to limit the scope of  
25           the claimed invention in any way. Numerous additional embodiments within the scope and spirit of the invention will become readily apparent to those skilled in the art.

In the examples below, the synthesized polymers were characterized via differential scanning calorimetry (DSC), gel permeation chromatography (GPC), and nuclear magnetic resonance (NMR) spectroscopy. DSC measurements were performed on a 2920 Modulated Differential Scanning Calorimeter from TA Instruments using aluminum sample pans and sample weights of 5-10 milligrams. Samples were heated from room temperature to 100°C at 10°C/minute; quenched to -40°C at 30°C/minute followed by heating to 100°C at 10°C/minute. For GPC, a Waters System with Millennium 32 Software and a 410 Refractive Index Detector were used. Molecular weights were determined relative to polystyrene standards using THF as the solvent. Proton NMR was obtained in deuterated chloroform on a 400MHz NMR spectrometer using Varian software.

**Example 1: Synthesis of a copolymer of monooleoyl glyceride and maleic anhydride**

142.6 grams of monooleoyl glycerol were added to a dry 250 ml, single neck, round bottom flask. A stir bar was added and a nitrogen inlet adapter was attached. The reaction flask was placed in a room temperature oil bath and a nitrogen gas blanket was started. The flask was heated to 140°C, and 39.2 grams of maleic anhydride were added. The temperature was raised to 190°C and maintained for 3 hours. After 3 hours the flask was removed from the oil bath to cool to room temperature.

The polymer was a pale yellow, viscous liquid. GPC measurement determined a number average molecular weight of 1383, and a weight average molecular weight of 6435.

5

**Example 2:** Synthesis of copolymer of monooleoyl glyceride and maleic anhydride and 5 mol% PEG400

40.1 grams of monooleoyl glycerol and 5.0 grams of PEG400 were added to a dry 100 ml, single neck, round bottom flask. A stir bar was added and a nitrogen inlet adapter was attached. The reaction flask was placed into a room temperature oil bath and a nitrogen blanket was applied. The oil bath temperature was raised to 140°C. Once at 140°C, 12.3 grams of maleic anhydride were added. The temperature was raised to 180°C and maintained for 7 hours at 180°C. The flask was removed from the oil bath and allowed to cool to room temperature. The polymer was a pale yellow, viscous liquid.

15  
20

GPC measurement determined a number average molecular weight of 1122, and a weight average molecular weight of 5647.

**Example 3:** Synthesis of copolymer of monooleoyl glyceride and maleic anhydride and 25 mol% PEG400

25

17.8 grams of monooleoyl glycerol and 20.0 grams of PEG400 were added to a dry 100 ml, single neck, round bottom flask. A stir bar was added and a nitrogen inlet adapter was attached. The reaction flask was placed into

a room temperature oil bath and a nitrogen blanket was applied. The oil bath temperature was raised to 140°C. Once at 140°C, 9.8 grams of maleic anhydride were added. The temperature was raised to 180°C and maintained for 7  
5 hours at 180°C. The flask was removed from the oil bath and allowed to cool to room temperature. The polymer was a pale yellow, viscous liquid.

GPC measurement determined a number average  
molecular weight of 1230, and a weight average molecular  
10 weight of 4481.

**Example 4:** Reaction of mercaptoethanol with copolymer of monooleoyl glyceride and maleic anhydride

5.0 grams of a copolymer of monooleoyl glyceride  
15 and maleic anhydride made following the procedure of Example 1, 0.77 ml of mercaptoethanol and 11 ml of DMF were added to a dry 50 ml, single neck, round bottom flask along with 52 milligrams of azobis  
isobutyronitrile (AIBN). A stir bar was added and a  
20 nitrogen inlet adapter was attached. The reaction flask was placed in a room temperature oil bath and a nitrogen blanket was started. The temperature was raised to 60°C and maintained for 24 hours. After 24 hours, the flask was removed from the oil bath to cool to room  
25 temperature. The polymer was diluted with 10 mL of ethyl acetate and then washed twice with an aqueous NaCl solution, dried with MgSO<sub>4</sub>, and filtered through a filter paper. The solvent was removed by rotary

evaporation followed by vacuum drying. The polymer was a yellow, transparent viscous liquid.

<sup>1</sup>H NMR showed that there was no  $\alpha,\beta$ -unsaturated ester remaining in the polymer (no peak at 6.8 ppm). <sup>1</sup>H NMR (400MHz, CD<sub>3</sub>Cl, ppm):  $\delta$  0.86 triplet (3H), 1.26 multiplet (22H), 1.61 multiplet (2H), 2.00 multiplet (4H), 2.30 multiplet (2H), 2.80 multiplet (3H), 3.00 doublet (2H), 3.80 multiplet (2H), 4.20 multiplet (5H), 5.38 multiplet (2H), 8.00 singlet (1H). IR confirms the presence of hydroxy functional groups. IR (ZnS): 3442, 2920, 2860, 1745, 1456, 1168 cm<sup>-1</sup>.

**Example 5:** Reaction of mercaptopropionic acid with copolymer of monooleoyl glyceride and maleic anhydride

5.0 grams of copolymer of monooleoyl glyceride and maleic anhydride made following the procedure of Example 1, 0.98 ml of mercaptopropionic acid, and 11 ml of DMF were added to a dry 50 ml, single neck, round bottom flask along with 54 mg (or 3 mole percent) of AIBN. A stir bar was added and a nitrogen inlet adapter was attached. The reaction flask was placed in a room temperature oil bath and a nitrogen blanket was started. The temperature was raised to 60°C and maintained for 24 hours. After 24 hours, the flask was removed from the oil bath to cool to room temperature. The polymer was diluted with 10 ml of ethyl acetate, washed with 0.01M NaOH, and then washed twice with an aqueous NaCl solution, dried with MgSO<sub>4</sub>, and filtered through a

filter paper. The solvent was removed by rotary evaporation followed by vacuum drying. The polymer was a yellow, transparent viscous liquid.

<sup>1</sup>H NMR showed that there was no  $\alpha,\beta$ -unsaturated ester remaining in the polymer (no peak at 6.8 ppm). <sup>1</sup>H NMR (400MHz, CD<sub>3</sub>Cl, ppm):  $\delta$  0.86 triplet (3H), 1.26 multiplet (22H), 1.45 multiplet (3H), 1.61 multiplet (2H), 2.00 multiplet (4H), 2.30 multiplet (2H), 2.90 multiplet (3H), 3.00 doublet (2H), 3.70 multiplet (2H), 4.20 multiplet (5H), 5.38 multiplet (2H), 8.00 singlet (1H). IR confirms the presence of hydroxy functional groups. IR (ZnS): 3437, 3213, 2920, 2860, 1745, 1456, 1168 cm<sup>-1</sup>.

**Example 6:** Reaction of mercaptoethylamine with copolymer of monooleoyl glyceride and maleic anhydride

5.0 grams of copolymer of monooleoyl glyceride and maleic anhydride made following the procedure of Example 1, 0.85 ml of mercaptoethylamine and 11 ml of DMF were added to a dry 50 ml, single neck, round bottom flask along with 54 mg of AIBN. A stir bar was added and a nitrogen inlet adapter was attached. The reaction flask was placed in a room temperature oil bath and a nitrogen blanket was started. The temperature was raised to 60°C and maintained for 24 hours. After 24 hours, the flask was removed from the oil bath to cool to room temperature. The polymer was diluted with 10 ml of ethyl acetate, washed with 0.01M NaOH, and then washed

twice with an aqueous NaCl solution, dried with MgSO<sub>4</sub>, and filtered through a filter paper. The solvent was removed by rotary evaporation followed by vacuum drying.

The polymer was a yellow, transparent viscous liquid.

5           <sup>1</sup>H NMR showed that there was no α,β-unsaturated ester remaining in the polymer (no peak at 6.8 ppm). <sup>1</sup>H NMR (400MHz, CD<sub>3</sub>Cl, ppm): δ 0.86 triplet (3H), 1.26 multiplet (22H), 1.61 multiplet (2H), 2.00 multiplet (4H), 2.30 multiplet (2H), 2.80 multiplet (2H), 3.60  
10 multiplet (2H), 4.20 multiplet (3H), 5.38 multiplet (2H). IR confirms the presence of amine functional groups. IR (ZnS): 3346, 2920, 2860, 1745, 1660, 1456, 1168 cm<sup>-1</sup>.

15       **Example 7:** Reaction of O-(2-aminoethyl)-O'-methylpolyethyleneglycol 5000 with copolymer of monooleoyl glycerol and maleic anhydride

          1.0 gram of poly(glyceryl monooleate-succinate), 11.1g of O-(2-aminoethyl)-O'-methylpolyethyleneglycol  
20 5000, and 11 ml of DMF were added to a dry 50 ml, single neck, round bottom flask along with 10.8 milligrams of AIBN. A stir bar was added and a nitrogen inlet adapter was attached. The reaction flask was placed in a room temperature oil bath and a nitrogen blanket was started.

25       The temperature was raised to 60°C and maintained for 24 hours. After 24 hours, the flask was removed from the oil bath to cool to room temperature. The polymer was diluted with 10 ml of ethyl acetate and then washed

twice with an aqueous NaCl solution, dried with MgSO<sub>4</sub>, and filtered through a filter paper. The solvent was removed by rotary evaporation followed by vacuum drying. The polymer was a white solid.

5           <sup>1</sup>H NMR showed that there was no α,β-unsaturated ester remaining in the polymer (no peak at 6.8 ppm). <sup>1</sup>H NMR (400MHz, CD<sub>3</sub>Cl, ppm): δ 0.86 triplet (3H), 1.26 multiplet (22H), 1.61 multiplet (2H), 2.00 multiplet (4H), 2.20 multiplet (22H), 3.60 multiplet (400H), 5.38  
10 multiplet (2H). IR (ZnS): 3473, 2860, 1745, 1456, 1342, 1282, 1242, 1113, 968, 844 cm<sup>-1</sup>.

**CLAIMS:**

1. A synthetic polymer comprising the reaction product of:

an  $\alpha,\beta$ -unsaturated polybasic acid or a derivative thereof; elected from anhydrides, mixed anhydrides, esters activated esters and acid halides and a mono glyceride;

and further comprising pended thereto a functional agent comprising a first functional nucleophilic moiety and a second functional moiety other than said first functional moiety.

2. The polymer of claim 1 wherein said  $\alpha,\beta$ -unsaturated polybasic acid is maleic acid, fumaric acid, citraconic acid or itaconic acid.

3. The polymer of claim 2 wherein said  $\alpha,\beta$ -unsaturated polybasic acid derivative is maleic anhydride.

4. The polymer of claim 2 wherein said  $\alpha,\beta$ -unsaturated polybasic acid is maleic acid.

5. The polymer of any one of claims 1 to 4 wherein said monoglyceride is monostearoyl glycerol, monopalmitoyl glycerol, monomyristoyl glycerol, monocaproyl glycerol, monodecanoyl glycerol, monolauroyl glycerol, monolinoleoyl glycerol or monooleoyl glycerol.

6. The polymer of any one of claims 1 to 5 wherein said functional agent is mercaptoethanol, mercaptopropanol, mercaptobutanol, mercaptohexanol, mercaptopropanediol, mercaptoacetic acid, mercaptopropionic acid, mercaptosuccinic acid or mercaptoethylamine.

7. The polymer of any one of claims 1 to 6 wherein said polymer is branched.

8. The polymer of any one of claims 1 to 7 wherein said polymer comprises the reaction product of said monoglyceride, and at least two of said  $\alpha,\beta$ -unsaturated polybasic acids or derivatives thereof selected from anhydrides, mixed anhydrides, esters activated esters and acid halides.

9. The polymer of any one of claims 1 to 7 wherein said polymer comprises the reaction product of said  $\alpha,\beta$ -unsaturated polybasic acid or a derivative thereof selected from anhydrides, mixed anhydrides esters, activated esters and acid halides, and at least two monoglycerides.

10. The polymer of any one of claims 1 to 9 wherein said polymer comprises the reaction product of said monoglyceride, said  $\alpha,\beta$ -unsaturated polybasic acid or derivative thereof, and a polybasic acid selected from the group consisting of succinic acid, glutaric acid, adipic acid, pimelic acid, suberic acid and sebacic acid.

11. A composition, comprising: a synthetic, biodegradable, biocompatible polymer according to any one of claims 1 to 10

12. The composition of claim 11 further comprising an effective amount of a bioactive agent.

13. The composition of claim 12 wherein said bioactive agent is selected from the group consisting of antiinfectives, analgesics, anorexics, antihelmintics, antiarthritics, antiasthmatics, anticonvulsants,

antidepressants, antidiuretics, antidiarrheals, antihistamines, antiinflammatory agents, antimigraine preparations, antinauseants, antineoplastics, antiparkinsonism drugs, antipruritics, antipsychotics, antipyretics, antispasmodics, anticholinergics, sympathomimetics, xanthine derivatives, calcium channel blockers, beta-blockers, antiarrhythmics, antihypertensives, diuretics, vasodilators, central nervous system stimulants, decongestants, hormones, steroids, hypnotics, immunosuppressives, muscle relaxants, parasympatholytics, psychostimulants, sedatives, tranquilizers, naturally derived or genetically engineered proteins, growth factors, polysaccharides, glycoproteins, or lipoproteins, oligonucleotides, antibodies, antigens, cholinergics, chemotherapeutics, hemostatics, clot dissolving agents, radioactive agents and cystostatics.

14. The composition of any one of claims 11 to 13 comprising a microdispersion, said microdispersion comprising a solid polymer dispersed in a liquid polymer, wherein one of said solid polymer or said liquid polymer comprises the synthetic polymer of any one of claims 1 to 10;

wherein said solid polymer has a melting point between 25°C and 70°C, and wherein said liquid polymer has a melting point below about 25°C.

15. The composition of claim 14 wherein both said solid polymer and said liquid polymer comprises a synthetic polymer according to any one of claims 1 to 10.

16. A medical device comprising a coating of a synthetic, biodegradable, biocompatible polymer according to any one of claims 1 to 10.

17. The medical device of claim 16, further comprising an effective amount of a bioactive agent.

18. The medical device of claim 16 or claim 17 further comprising an aliphatic polyester prepared from glycolide, L-lactide, D-lactide, meso-lactide, rac-lactide, epsilon - caprolactone, trimethylene carbonate, p-dioxanone, 1,4-dioxanone, 1,4-dioxepan-2-one, 1,5-dioxepan-2-one and/or a substituted derivative thereof.

19. The medical device of any one of claims 16 to 18 which is a suture anchor, sutures, staple, surgical tack, clip, plate, screw, drug-delivery device, adhesion prevention film or foam or a tissue adhesive.