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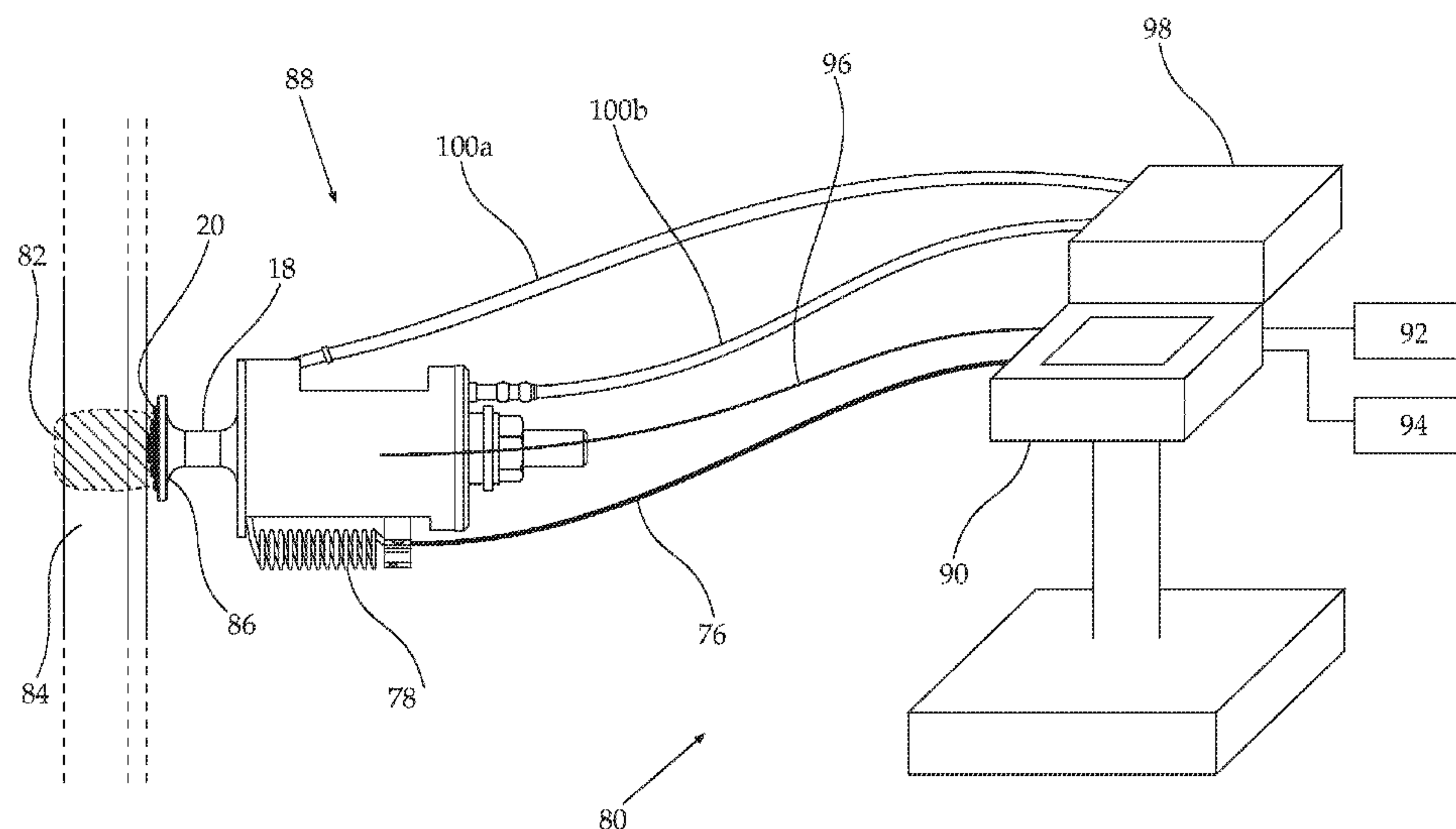
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(54) Title: CONCURRENT TREATMENT WITH THERMAL AND ACOUSTIC ENERGY



(57) **Abrégé/Abstract:**

Disclosed are methods for treating a volume of material by concurrently conveying acoustic energy and depositing thermal energy using a unipolar RF (radio-frequency) field. Also disclosed are devices suitable for concurrently conveying acoustic energy and depositing thermal energy using a unipolar RF (radio-frequency) field into the same volume of material. In some embodiments, the disclosed methods and devices are implemented for the treatment of subcutaneous fat.

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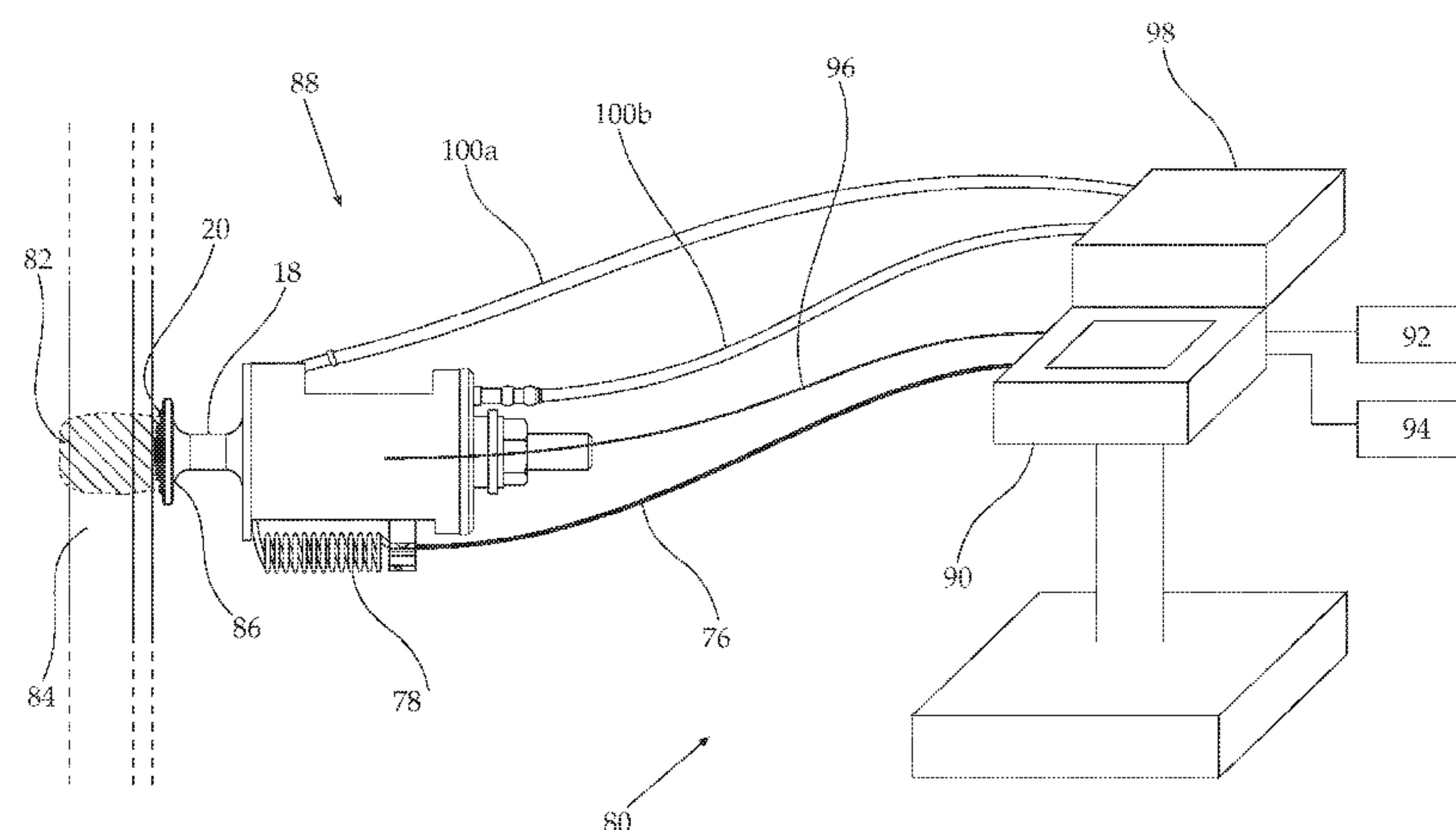


FIG. 2

(57) Abstract: Disclosed are methods for treating a volume of material by concurrently conveying acoustic energy and depositing thermal energy using a unipolar RF (radio-frequency) field. Also disclosed are devices suitable for concurrently conveying acoustic energy and depositing thermal energy using a unipolar RF (radio-frequency) field into the same volume of material. In some embodiments, the disclosed methods and devices are implemented for the treatment of subcutaneous fat.

CA-2,836,706

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CONCURRENT TREATMENT WITH THERMAL AND ACOUSTIC ENERGY**RELATED APPLICATIONS**

The present application takes priority from US Provisional Patent Application 61/487,720 filed 19 May 2011.

FIELD AND BACKGROUND OF THE INVENTION

The invention, in some embodiments, relates to the field of treatment of body tissue with energy, and more particularly, but not exclusively, to methods and devices for treatment of subcutaneous fat using a combination of thermal energy deposited using a unipolar RF (radio-frequency) field and acoustic energy, for example for subcutaneous fat reduction.

Adipose tissue comprises primarily adipocytes containing fat together with fibroblasts, macrophages and endothelial cells. In mammals such as humans, one of the main locations of adipose tissue is the hypodermis (subcutaneous tissue) located beneath the skin (epidermis and dermis) that insulates the body core from external temperature changes but most importantly acts as an energy store for the mammal.

Unlike excessive visceral fat, excessive subcutaneous fat (fat in the hypodermis) in humans is not directly associated with pathologies. However, excessive subcutaneous fat is considered to be unaesthetic and it is common for people to try to reduce the amount and distribution of subcutaneous fat to achieve a more aesthetic external appearance. It is often preferred to treat subcutaneous fat by the local application of energy. Specifically, over a series of individual sessions, energy is locally-applied to the hypodermis. Such local application of energy over a series of individual sessions allows different amounts of subcutaneous fat to be removed from the hypodermis at different locations of the body, allowing the body to be shaped to achieve a desired aesthetic appearance.

Treatment of subcutaneous fat with acoustic energy

One popular mode of locally-applied energy for the treatment of subcutaneous fat is conveying of acoustic energy (for example, using acoustic waves) through a skin layer into the hypodermis, for example as described in patent application publication US 2011/0213279 of the Applicant, as well as the references cited therein. The acoustic radiative surface of a sonotrode functionally associated with an ultrasound transducer is coupled (e.g., by direct contact or by indirect contact through a coupling substance, e.g., a liquid or gel) to a skin surface of a subject to be

treated. The ultrasound transducer is activated to generate acoustic waves that are directed by the acoustic radiative surface of the sonotrode through the skin surface to convey acoustic energy into a volume of the hypodermis. It is believed that application of sufficient acoustic energy (in terms of power, intensity and duration) damages and even ruptures the walls of adipocytes in the hypodermis, releasing fat contained therein into the bulk of the hypodermis.

The power of the acoustic waves is chosen so that the acoustic waves convey substantial energy to a depth of about 2 cm past the skin surface. By "substantial energy" is meant sufficient to achieve a desired result in the treatment of subcutaneous fat. Although acoustic compression (longitudinal) waves are typically used, it has been found that acoustic shear (transverse) waves are also effective, as discussed in US 2011/0213279.

Typically, a course of treatment of subcutaneous fat with acoustic energy includes about six individual weekly treatment sessions. In the period between any two individual sessions, the body clears the fat and cell debris released into the bulk of the hypodermis. To treat an area the size of two thighs and a belly, each session has a duration of about 1 hour which is often considered excessively long, tiring both the treated subject and the operator. The only solution for reducing the duration of an individual session is by increasing the power of the acoustic waves and thereby of the acoustic energy conveyed into the hypodermis. However, increasing the power typically leads to deeper penetration into the body of the treated subject which can be dangerous and damaging to other tissue.

Treatment of subcutaneous fat with thermal energy

Another popular mode of locally-applied energy for the treatment of subcutaneous fat is heating of a volume of the hypodermis by depositing thermal energy by application of RF (radio-frequency) waves through the skin. The manner in which applied RF waves deposit thermal energy into a volume of hypodermis, and the physiological effect such depositing has, depends on the frequency of the RF waves and the manner in which applied.

RF waves that produce electrical current

One manner of applying RF waves to treat subcutaneous fat is to produce an electric current (ionic movement) in the hypodermis between two electrodes, see for example, US 2007/0239075 or US 6,662,054. Specifically, two electrodes are coupled (e.g., by direct contact or by indirect contact through a coupling substance, e.g., a liquid or gel) with a skin surface and a functionally-associated RF energy source is activated, producing an RF current that passes through the tissue between the two electrodes. Tissue between the electrodes

through which the current passes is heated primarily as a result of the electrical resistance of the tissue.

There are a number of limitations of applying RF waves to deposit thermal energy to treat subcutaneous fat by producing an RF current that passes therethrough.

5 Indiscriminately passing electric current through the body of a person is dangerous and can lead to electrocution or disruption of heart function. Since electrical current passes between the two electrodes, in practical implementations of such methods the two electrodes are maintained close together (typically between 1 and 5 cm) to ensure that the current-path is well-defined and benign.

10 Generally, the lower the frequency of the RF waves, the more effectively the thermal energy is deposited by the produced RF current passing through the tissue.

It is generally accepted that for depositing thermal energy using such an RF current, RF frequencies up to about 2 MHz are effective and that RF frequencies above 200 MHz provide substantially no heating. The efficacy of depositing thermal energy with a produced
15 RF current falls-off quickly from frequencies of 2 MHz to about 200 MHz. That said, medical regulatory requirements and legal limitations on RF transmission restrict frequencies used in medical treatments to frequencies in the Industrial, Scientific and Medical (ISM) bands. The ISM bands are typically higher than ideal for depositing thermal energy by a current as described above, e.g., 13.560 MHz $\pm$ 7 kHz, 27.120 MHz $\pm$ 163 kHz, 40.68 MHz $\pm$
20 20 kHz and, in some localities, 6.780 MHz $\pm$ 15 kHz. Thus, effective implementation of such methods is practically limited to the lower ISM frequency of 6.780 MHz $\pm$ 15 kHz and possibly 13.560 MHz $\pm$ 7 kHz, while at the higher ISM frequencies 27.120 MHz $\pm$ 163 kHz and 40.68 MHz $\pm$ 20 kHz, such methods are inefficient.

The maximal power of the electric current produced as described above is limited by
25 the power that ensures that the skin surface suffers no substantial damage (e.g., burning, ablation), thereby also limiting the inter-electrode distance and the degree of heating of hypodermis that can be achieved using such methods.

The hypodermis, especially a hypodermis containing excessive fat, has a conductivity an order of magnitude lower than that of skin. As a result, most of the current produced as
30 described above passes through the skin and very little current, and therefore power for heating, passes through the hypodermis.

The current that does pass through the hypodermis passes only through the upper few millimeters of the hypodermis and does not lead to substantial deposition of thermal energy deeper in the hypodermis. As noted above, it is not practically possible to increase the

amount and depth of thermal energy deposition by increasing the power of the current without damaging the skin.

Despite the severe limitation on the power of the current that can be produced in the hypodermis as described above and the concomitant limitation of the amount of thermal energy deposited, such methods have proven to be not totally ineffective in treating subcutaneous fat in the upper part of the hypodermis due to the structure of the hypodermis. Specifically, a volume of hypodermis comprises mostly poorly conductive adipocytes, substantially globules of poorly-conducting fat with a small amount of conductive cytoplasm surrounded by electrically insulating cell walls, and between the adipocytes a relatively small amount of conductive intercellular fluid. As a result, electric current produced in the hypodermis passes almost entirely through the intercellular fluid. Since the current is limited to the small volume of the intercellular fluid, despite the relatively low current the concomitant local heating is to a relatively high temperature (typically above 65 °C) that is sufficient to substantially damage adjacent adipocyte walls leading to necrosis or apoptosis thereof.

One solution proposed to deposit thermal energy to treat subcutaneous fat found deeper in the hypodermis as well as to drive less current through the skin and more through the hypodermis is to place the two electrodes on either side of a fold of tissue including the skin and hypodermis, see for example, US 2007/0239075 or US 6,662,054. Clearly, such a treatment that includes folding tissue, for example by suction, is unpleasant for both the subject and the person performing the treatment, is not applicable to all body surfaces, and is of limited efficacy.

An interesting variant for the treatment of subcutaneous fat has been described in US 2007/0239075 which teaches a treatment combining acoustic energy and deposited thermal energy by using RF waves between two electrodes to produce a current in the hypodermis as described above. Therein is reported that the combined cell-wall destroying effects of the two types of energy are particularly effective. The combined treatment still suffers from disadvantages, for example, the inability for treatment of deeper layers of the hypodermis except by folding tissue with the concomitant disadvantages as described above.

Dielectric heating with RF waves

Another manner of applying RF waves to treat subcutaneous fat is through dielectric heating to deposit thermal energy directly into a volume of tissue with a unipolar RF field, for instance, as described in US 7,630,774 of the Applicant

if fully set forth herein. An RF applicator including an RF radiative surface is coupled (e.g., contacted) with a skin surface and a RF energy source functionally-associated therewith is activated to produce RF waves. The RF applicator directs RF waves generated by an activated RF energy source to the RF radiative surface to form a unipolar RF field that passes
5 through skin with which the RF radiative surface is coupled. The formed RF field causes dipolar molecules in the tissue, such as water, to rotate thereby depositing thermal energy in the volume of tissue. It is important to note that at lower frequencies a unipolar RF field may also deposit some thermal energy in tissue by other modes, for example by a current related to polarization of the tissue. Such other modes are more significant the lower the frequency of
10 the RF field: progressively less important at greater than 2 MHz, and being insubstantial at frequencies greater than 10 MHz.

Compared to other tissue such as skin and muscle, the hypodermis includes relatively few blood vessels and is therefore not effectively cooled by the body. Typically dielectric heating with a unipolar RF field allows deposition of thermal energy sufficient to raise the
15 temperature of a volume of tissue to about 45°C - 48°C. Although no direct damage is done to the adipocytes in the hypodermis by such heating (as opposed to heating resulting from a current produced as described above), apparently such a temperature increase is sufficient to raise the metabolic rate in the hypodermis to an extent that allows reduction of the amount of fat in the hypodermis, for example, by increasing the rate of flow of bodily fluids through the
20 heated volume of tissue.

In dielectric heating with a unipolar RF field, the greater the power of the RF waves, the deeper the RF field penetrates and consequently, the deeper thermal energy is deposited. Accordingly, the maximal power of the RF waves for dielectric heating is limited to a power that ensures that no substantial damage is done to tissue deeper than the hypodermis. That
25 said, dielectric heating allows treatment of subcutaneous fat in the entire hypodermis (typically to a maximal depth of about 2 cm) and not only in the upper layers thereof as in heating by a produced current as discussed above.

For dielectric heating, the efficiency (proportion of power of the RF waves to thermal energy deposited in the tissue) increases with increasing frequency. Thus although any
30 frequency can be used for dielectric heating of tissue, typically an RF field having a frequency of at least 2 MHz, at least 4MHz and even at least 10 MHz is preferred. That said, dielectric heating of hypodermis with a unipolar RF field is most effective at frequencies between 10 MHz and 100 MHz, especially at higher values of this range.

As with treatment with acoustic energy, a typical course of treatment of subcutaneous fat with RF waves, whether for dielectric heating or for heating by an induced current, includes about six individual weekly treatment sessions. To treat an area the size of two thighs and a stomach, each such individual session has a duration of about 1 hour.

5 Analogously to treatment with acoustic energy, the only manner of reducing the duration of a given individual session is by increasing the power of the RF energy source which, as discussed above, is not practical.

It has been proposed during an individual treatment session to first treat a volume of tissue with acoustic energy to damage adipocyte walls and then to deposit thermal energy in
10 the same volume of tissue by dielectric heating to accelerate local metabolism to clear the fat and cell debris released into the volume of tissue by the acoustic energy treatment. In a single such combined session to treat an area the size of two thighs and a belly, the duration of the acoustic treatment is about 1 hour followed by dielectric heating for about 20 to 30 minutes. It has been found that although each such session is of longer duration; such combined
15 treatments provide better results.

SUMMARY OF THE INVENTION

The invention, in some embodiments, relates to the treatment of body tissue with energy and more particularly, but not exclusively, to methods for the treatment of tissue such
20 as subcutaneous fat using a combination of thermal energy and acoustic energy. The invention, in some embodiments, relates to devices for treatment of material with energy and more particularly, but not exclusively, to a device suitable for the treatment of a volume of material with a combination of thermal energy and acoustic energy, for example materials such as hypodermis, especially for the treatment of subcutaneous fat.

25 Thus, according to an aspect of some embodiments of the invention there is provided a method of treatment of subcutaneous fat in a subject, comprising: concurrently

a) conveying an effective amount of acoustic energy into a volume of hypodermis through a skin surface with which an acoustic radiative surface of a sonotrode is coupled; and

b) depositing an effective amount of thermal energy into the volume of hypodermis
30 with a unipolar RF field through a skin surface.

According to an aspect of some embodiments of the invention there is also provided a device suitable for treatment of a volume of material with energy through a surface, the device comprising:

an ultrasound transducer functionally associated with a sonotrode having an acoustic radiative surface, the ultrasound transducer configured, when activated, to generate acoustic waves that are directed by the acoustic radiative surface into the volume of material through a first portion of a surface with which the acoustic radiative surface is coupled to convey an effective amount of acoustic energy into the volume of material; and

an RF (radio-frequency) applicator having an RF radiative surface, which RF applicator is functionally associable with an RF energy source, the RF applicator configured to direct RF waves, generated by an activated RF energy source functionally-associated with the RF applicator, to the RF radiative surface to form a unipolar RF field, the unipolar RF field passing through a second portion of the surface with which the RF radiative surface is coupled to deposit an effective amount of thermal energy in the volume of material, wherein the device is configured for concurrent depositing of the effective amount of thermal energy and conveying of the effective amount of acoustic energy into the volume of material.

Unless otherwise defined, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which the invention pertains. In case of conflict, the specification, including definitions, will control.

As used herein, the terms "comprising", "including", "having" and grammatical variants thereof are to be taken as specifying the stated features, integers, steps or components but do not preclude the addition of one or more additional features, integers, steps, components or groups thereof. These terms encompass the terms "consisting of" and "consisting essentially of".

As used herein, the indefinite articles "a" and "an" mean "at least one" or "one or more" unless the context clearly dictates otherwise.

As used herein, in some instances (for example in US Provisional Patent Application 61/487,720) the terms "*ultrasound radiative surface*" and "*ultrasonic radiative surface*" and variants thereof are substantially synonymous with the term "*acoustic radiative surface*" and variants thereof.

As used herein, in some instances (for example in US 61/487,720) the phrase "*to deliver an effective amount of ultrasonic (mechanical) waves into a volume of material*" and variants thereof is substantially synonymous with the phrase "*to convey an effective amount of acoustic energy into a volume of material*" and variants thereof.

As used herein, in some instances (for example in US 61/487,720) the phrase "*to direct an RF alternating electric field into a volume of material so that the RF alternating*"

electric field conveys an effective amount of energy in the volume of material" and variants thereof is substantially synonymous with the phrase *"to deposit an effective amount of thermal energy into a volume of material"* and variants thereof.

5 BRIEF DESCRIPTION OF THE FIGURES

Some embodiments of the invention are described herein with reference to the accompanying figures. The description, together with the figures, makes apparent to a person having ordinary skill in the art how some embodiments of the invention may be practiced. The figures are for the purpose of illustrative discussion and no attempt is made to show structural details of an embodiment in more detail than is necessary for a fundamental understanding of the invention. For the sake of clarity, some objects depicted in the figures are not to scale.

In the Figures:

FIG. 1A depicts an embodiment of a device suitable for treatment of a volume of material such as hypodermis according to the teachings herein fully assembled, in perspective from a distal end;

FIG. 1B depicts the embodiment of the device of Figure 1A fully assembled, in perspective from a proximal end;

FIG. 1C depicts the embodiment of the device of Figures 1A and 1B, with some components removed to show details of construction from the side;

FIG. 1D depicts the embodiment of the device of Figures 1A-1C, with some components removed to show details of construction, in perspective from a distal end;

FIG. 1E depicts the embodiment of the device of Figures 1A-1D, with some components removed to show details of construction, in perspective from a distal end;

FIG. 1F depicts the embodiment of the device of Figures 1A-1E, with some components removed to show details of construction, in perspective from a proximal end; and

FIG. 2 schematically depicts a second embodiment of a device suitable for treatment of a volume of material such as hypodermis according to the teachings herein.

30 DESCRIPTION OF SOME EMBODIMENTS OF THE INVENTION

The invention, in some embodiments, relates to the treatment of body tissue with energy and more particularly, but not exclusively, to methods for the treatment of tissue such as subcutaneous fat using a combination of thermal energy and acoustic energy. The invention, in some embodiments, relates to devices for treatment of material with energy and

more particularly, but not exclusively, to a device suitable for the treatment of a volume of material with a combination of thermal energy and acoustic energy, for example materials such as hypodermis, especially subcutaneous fat.

The principles, uses and implementations of the teachings herein may be better understood with reference to the accompanying description and figures. Upon perusal of the description and figures present herein, one skilled in the art is able to implement the invention without undue effort or experimentation. In the figures, like reference numerals refer to like parts throughout.

Before explaining at least one embodiment in detail, it is to be understood that the invention is not necessarily limited in its application to the details of construction and the arrangement of the components and/or methods set forth herein. The invention is capable of other embodiments or of being practiced or carried out in various ways. The phraseology and terminology employed herein are for descriptive purpose and should not be regarded as limiting.

As discussed above, it is known to use acoustic energy to treat subcutaneous fat by conveying acoustic energy using acoustic waves through the skin into the hypodermis, see for example US 2011/0213279. It is also known to deposit thermal energy into a volume of tissue through dielectric heating with a unipolar RF field to treat subcutaneous fat, see for example US 7,630,774. Such treatments take an excessively long time: as discussed above, a treatment session of an area the size of two thighs and a belly typically takes about an hour.

Increasing the power of such treatments is potentially unsafe, including the possibility of causing excessive damage, including to tissue other than the hypodermis.

As noted above in the introduction, it has been found that serially combining the two treatments, e.g., acoustic energy treatment followed by thermal energy treatment yields improved results but no significant savings in time: as discussed above, such a serial treatment session of an area the size of two thighs and a stomach typically takes about 90 minutes.

Method of treatment of subcutaneous fat

According to an aspect of some embodiments of the teachings herein, there is provided a method of treatment of subcutaneous fat in a subject, comprising: concurrently

a) conveying an effective amount of acoustic energy, for example, generated by an ultrasound transducer, into a volume of hypodermis through a skin surface with which an acoustic radiative surface of a sonotrode is coupled; and

b) depositing an effective amount of thermal energy into the volume of hypodermis with a unipolar RF field through a skin surface, so that the heating is primarily by dielectric heating. In some embodiments, the subject is a human. In some embodiments, the subject is a non-human animal.

5 In some embodiments, conveying of the effective amount of acoustic energy concurrently with the depositing of the effective amount of thermal energy initiates a process leading to a reduction of the amount of fat in the volume of hypodermis.

In some embodiments, the depositing of the effective amount of thermal energy is sufficient to substantially raise (and in some embodiments maintain) the temperature of the
10 volume of hypodermis to a temperature of between 42°C and 48°C, and in some embodiments between 42°C and 46°C.

Typically, the method is non-invasive, that is to say the skin surface remains intact, and is not punctured or otherwise penetrated. In some embodiments, the method is a non-surgical method, performed without breaking the skin. Embodiments of the method are
15 performed by any suitable person, including medical personnel but typically aesthetic technicians such as beauticians.

In some embodiments, the concurrent exposure of the same volume of hypodermis to both acoustic energy and thermal energy leads to greater efficacy and/or (surprisingly) shorter treatment times when compared to equivalent treatments by thermal energy alone, acoustic
20 energy alone or serial treatment as described above. For example, in some embodiments, the concurrent exposure of the same volume of a subcutaneous fat layer to both acoustic energy and thermal energy leads to faster treatment for similar effect (e.g., each session of around 30 to 35 minutes instead of 60 minutes) without requiring an increase of power of either modality.

25 In some embodiments, it has been found that it is possible to reduce the power of the acoustic energy and/or of the RF field when compared to equivalent treatments by thermal energy alone, acoustic energy alone or serial treatment as described above and still achieve comparable or better effects.

Although not wishing to be held to any one theory, it is believed that in some
30 embodiments the walls of adipocytes that are at or maintained at higher than body temperatures (e.g., 42°C - 48°C, more typically 42°C - 46°C) are more susceptible to damage and disruption by acoustic energy (whether continuously or discontinuously applied acoustic energy) than adipocytes at body temperature.

Although not wishing to be held to any one theory, it is believed that in some embodiments the walls of adipocytes that are subject to repeated variations of temperature (e.g., within a range having a lower value at least of body temperature and an upper value of up to 48°C, more typically up to 46°C) are more susceptible to damage and disruption by
5 acoustic energy (whether continuously or discontinuously applied acoustic energy) than adipocytes maintained at a constant temperature, especially at a constant temperature near body temperature.

In some embodiments, the concurrent exposure of the same volume of hypodermis to both acoustic energy and thermal energy reduces unwanted side-effects apparent, for
10 example, when treating hypodermis with acoustic energy alone. For example, in some embodiments, the incidence of ovoid adipocytes or lipid lacunae, which appearance is known subsequent to treatment with acoustic energy alone, is reduced.

Generally, conveying acoustic energy into a volume of hypodermis through a skin surface occurs when an acoustic radiative surface of a sonotrode functionally associated with
15 an activated ultrasound transducer is coupled with a skin surface, e.g., the acoustic radiative surface is in direct contact with the skin, or is in indirect contact with the skin, for example, through an impedance-matching material such as an ultrasound gel (e.g., Graham-Field Ultrasound Gel, GF Health Products Inc., Atlanta, Georgia, USA) or petroleum jelly.

In some embodiments, the depositing of the effective amount of thermal energy into
20 the volume of hypodermis with a unipolar RF field is effected through a skin surface with which an RF radiative surface of an RF applicator is coupled (e.g., is in direct contact or is in indirect contact with the skin), the RF applicator directing RF waves generated, for example, by an activated RF energy source.

25 Volume of hypodermis

The volume of hypodermis to which concurrently an effective amount of acoustic energy is conveyed and an effective amount of thermal energy is deposited is of any suitable size. That said, in typical embodiments the volume is between 7 cm³ and 56 cm³, e.g., a 1 to 2
30 cm deep cylinder of tissue beneath a skin area of between 7 cm² (e.g., a circle having a radius of 1.5 cm) and 28 cm² (e.g., a circle having a radius of 3 cm).

In a manner analogous to that known in the art, during a treatment session of a subject in accordance with the method according to the teachings herein, the location of the volume of hypodermis to which an effective amount of acoustic energy is conveyed and concurrently an effective amount of thermal energy is deposited at any one time is changed, for example,

by moving an acoustic radiative surface and an RF radiative surface during a single session to couple to different portions of the skin surface of a subject. Accordingly, in some embodiments, a lubricant material is applied between the skin surface and the radiative surfaces. Often, such a lubricant is selected to also function as an impedance-matching material as noted above.

It is important to note that in some, but not all, embodiments of the method according to the teachings herein, the volume of hypodermis to which both the effective amount of acoustic energy is conveyed and the effective amount of thermal energy is deposited is smaller than the volume of hypodermis to which only an effective amount of acoustic energy is conveyed. Similarly, in some, but not all, embodiments of the method according to the teachings herein, the volume of hypodermis to which both the effective amount of acoustic energy is conveyed and the effective amount of thermal energy is deposited is smaller than the volume of hypodermis to which only an effective amount of thermal energy is deposited.

15 Shared radiative surfaces

In order to increase the intersection of the volume of hypodermis to which the effective amount of acoustic energy is conveyed with the volume of hypodermis in which the effective amount of thermal energy is deposited, in some embodiments, the ultrasound radiative surface and the RF radiative surface are at least partially shared, that is to say, at least a portion of the ultrasound radiative surface constitutes at least a portion of the RF radiative surface. In some such embodiments, at least a portion of the ultrasound radiative surface constitutes the RF radiative surface. In some such embodiments, at least a portion of the RF radiative surface constitutes the ultrasound radiative surface.

25 Same radiative surfaces

In some embodiments, the ultrasound radiative surface and the RF radiative surface are substantially the same radiative surface, that is to say, the ultrasound radiative surface constitutes the RF radiative surface. In such embodiments, the intersection between the volume of hypodermis to which an effective amount of acoustic energy is conveyed and the volume of hypodermis to which an effective amount of thermal energy is deposited is greatest. Further, the volume of hypodermis affected by only one of the two modalities is smallest, reducing the chance of undesired side effects, providing a more homogenous treatment and rendering the method more easily implementable.

Concurrent conveying of acoustic energy and depositing of thermal energy

The method of treating subcutaneous fat described herein comprises concurrently conveying an effective amount of acoustic energy and depositing an effective amount of thermal energy into a volume of hypodermis with a unipolar RF field.

5 *Simultaneous*

In some embodiments by concurrent is meant that the conveying of the effective amount of acoustic energy and the depositing of the effective amount of thermal energy is simultaneous.

10 In some such embodiments, during a period of time, the conveying of the effective amount of acoustic energy is continuous and the depositing of the effective amount of thermal energy is also continuous. It is believed that in such embodiments, the efficacy of the acoustic energy is increased because the volume of hypodermis is maintained at a temperature higher than body temperature.

15 In some such embodiments, during a period of time (e.g., a period of time having a duration of at least 10 seconds), the conveying of the effective amount of acoustic energy is continuous and the depositing of the effective amount of thermal energy is discontinuous (e.g., at irregular intervals, regular intervals, periodically). In some such embodiments, the depositing of the effective amount of thermal energy is during not less than 30% of the period of time and even not less than 45% of the period of time. In some such embodiments, the
20 effective amount of thermal energy is deposited periodically during the period of time at a rate not slower than 0.2 Hz. In some such embodiments, discontinuous depositing of thermal energy maintains the volume of hypodermis at an elevated (higher than body) temperature. In this context it is important to note that subcutaneous fat is typically less effectively cooled than other tissue such as skin, so that in some embodiments discontinuous depositing of
25 thermal energy allows maintenance of subcutaneous fat at elevated temperatures while reducing the chance that other tissue is adversely effected by the heating. That said, in some such embodiments, discontinuous depositing of thermal energy leads to repeated variations of temperature of the volume of hypodermis. It is believed that in some such embodiments, the efficacy of the conveyed acoustic energy is increased because the adipocytes in the volume of
30 tissue are subject to repeated variation of temperature.

Alternating

In some embodiments by concurrent is meant that the conveying of the effective amount of acoustic energy alternates with the depositing of the effective amount of thermal energy. In some such embodiments, the alternating is at a rate of not slower than 0.2 Hz. In

some embodiments, the alternating is at regular intervals, for example, periodic while in some embodiments, the alternating is at irregular intervals. In some such embodiments, such discontinuous depositing of thermal energy maintains the volume of hypodermis at an elevated temperature. Although it is generally accepted in the art that acoustic energy must be continuously conveyed to be effective, it is believed that in some such embodiments, the elevated temperature of the volume of hypodermis renders discontinuous conveying of the acoustic energy effective.

In some such embodiments, discontinuous depositing of thermal energy leads to repeated variations of temperature of the volume of hypodermis. Although it is generally accepted in the art that acoustic energy must be continuously conveyed to be effective, it is believed that in some such embodiments, the varying temperature of the volume of hypodermis renders the discontinuous conveying of the acoustic energy particularly effective.

It is important to note, that in some embodiments, as noted above, that discontinuous depositing of thermal energy reduces the incidence of unwanted side-effects such as burning of the skin without substantially reducing the efficacy of the treatment.

Effective amount of acoustic energy

By an effective amount of acoustic energy is meant intensity and duration of acoustic energy having suitable characteristics (e.g., direction, dispersion, frequency) to lead to a desired effect, such as damage to adipocytes in a hypodermis, e.g., for aesthetic modification. A person having ordinary skill in the art is familiar with or is able to decide or is able to determine without undue experimentation what constitutes an effective amount of acoustic energy in analogy to known commercially-available such treatments. In this context it is important to note that, in some embodiments of the method described herein, the intensity of the acoustic energy conveyed to the volume of hypodermis is reduced compared to comparable known treatments allowing a reduction of unwanted side effects such as unwanted damage to non-adipocyte cells.

Acoustic energy is conveyed with the use of acoustic waves. Acoustic waves having any suitable characteristics may be used in implementing embodiments of the method according to the teachings herein, especially acoustic waves having characteristics known in the art of the treatment of adipose tissue, especially subcutaneous fat such as discussed in US 2011/0213279. Such waves typically have a frequency of between 20 kHz and 100 kHz.

In some embodiments, the effective amount of acoustic energy is conveyed by longitudinal waves.

In some embodiments, the effective amount of acoustic energy is conveyed by transverse waves.

In some embodiments, the effective amount of acoustic energy is conveyed by both longitudinal and transverse waves.

- 5 In some embodiments, during a period of time that the method is implemented, the the effective amount of acoustic energy is alternately conveyed by longitudinal waves and by transverse waves.

Effective amount of thermal energy

- 10 By an effective amount of thermal energy is meant an amount of thermal energy that provides sufficient heating of the volume of hypodermis for an intended purpose, e.g., for aesthetic modification. A person having ordinary skill in the art is familiar with or is able to decide or is able to determine without undue experimentation what constitutes an effective amount of thermal energy, typically an amount of thermal energy sufficient to raise the
15 temperature in the volume of hypodermis to between 42°C and 48°C.

- In this context it is important to note that, in some embodiments of the method described herein, an equivalent desired effect is achieved when the temperature to which the volume of hypodermis is raised is lower than that of comparable known treatments, e.g., to between 42°C and 46°C, in some embodiments between 42°C and 45°C. In some
20 embodiments, such lower temperature is achieved by reducing the amount of the thermal energy deposited in the volume of hypodermis when compared to comparable known treatments, allowing a reduction of unwanted side effects such as burning of the skin and unwanted damage to non-adipocyte cells.

- To deposit the effective amount of thermal energy, a unipolar RF electric field having
25 any suitable characteristics (e.g., intensity, duration, frequency) is used in implementing embodiments of the method according to the teachings herein, especially a unipolar RF electric field having characteristics known in the art of the treatment of adipose tissue, especially subcutaneous fat layers such as discussed in US 7,630,774.

- A unipolar RF field having any suitable frequency may be used for depositing the
30 effective amount of thermal energy, typically a frequency between 3 Hz and 300 GHz. That said, since the preferred mode of depositing thermal energy, in some embodiments it is preferred that the unipolar RF field have a frequency of not less than 2 MHz, not less than 4 MHz and in some embodiments not less than 10 MHz. In typical preferred embodiments, the unipolar RF field has a frequency between 10 MHz and 100 MHz.

That said, due to legal limitations as well as proven efficacy in the field of treating adipose tissue, in some embodiments the unipolar RF field has a frequency in an Industrial, Scientific and Medical (ISM) frequency band. Accordingly, in some embodiments the unipolar RF field has a frequency in a frequency band selected from the group consisting of
 5 generally accepted ISM frequency bands (13.560 MHz $\pm$ 7 kHz, 27.120 MHz $\pm$ 163 kHz, 40.68 MHz $\pm$ 20 kHz, 2.45 GHz $\pm$ 50 MHz, 5.800 GHz $\pm$ 75 MHz, 24.125 GHz $\pm$ 125 MHz), frequencies that are subject to local acceptance (6.780 MHz $\pm$ 15kHz, 61.25 GHz $\pm$ 250 MHz, 122.5 GHz $\pm$ 500 MHz, 245 GHz $\pm$ 1 GHz), accepted in International Telecommunication Union Region 1 only (Europe, Asia, Africa, excluding the Far-East,
 10 Oceania and Australia; 433.92 MHz $\pm$ 870 kHz) and accepted in International Telecommunication Union Region 2 only (the Americas, 915 MHz $\pm$ 13 MHz). That said, in some embodiments the unipolar RF field has a frequency in a frequency band selected from the group of frequency typically used in the field of treatment of adipose tissue, 13.560 MHz $\pm$ 7 kHz, 27.120 MHz $\pm$ 163 kHz, 915 MHz $\pm$ 13 MHz, but most especially 40.68 MHz $\pm$ 20
 15 kHz.

Cooling of a skin surface

As is known in the art, depositing an effective amount of thermal energy into a volume of hypodermis through a skin surface to lead to a desired effect such as heating of the
 20 hypodermis can lead to undesirable effects such as burning or scorching the skin. Such undesirable effects may be aggravated by the concurrent (especially simultaneous) conveying of acoustic energy as disclosed herein.

In some embodiments, the characteristics of the unipolar RF field are selected to avoid undesirable effects, for example, in accordance with the teachings of US 7,630,774.

25 Alternatively or additionally, in some embodiments a portion of the skin surface of the subject is actively cooled.

In some embodiments, the method further comprises, during the depositing of an effective amount of thermal energy, cooling a portion of a skin surface proximal to the acoustic radiative surface, in some embodiments, thereby effecting cooling of a portion of a
 30 skin surface proximal to the acoustic radiative surface. In some such embodiments, the ultrasound radiative surface is cooled, for example by the passage of a cooling fluid in proximity thereto (for example near or through the sonotrode), to effect cooling of the portion of the skin surface.

In some embodiments, the method further comprises, during the depositing of an effective amount of thermal energy, cooling a portion of a skin surface proximal to the RF radiative surface, in some embodiments, thereby effecting cooling of a portion of a skin surface proximal to the RF radiative surface. In some such embodiments, the RF radiative surface is cooled, for example by the passage of a cooling fluid in proximity thereto (for example near or through the RF applicator), to effect cooling of the portion of the skin surface.

Use of impedance matching material

As known in the art, conveying acoustic energy into a volume of tissue such as hypodermis through a skin surface is most effective when contact with the skin is made with the help of an impedance matching material between the skin surface and the ultrasound radiative surface, for example with a fluid material that also acts as a lubricant such as an ultrasound gel (e.g., Graham-Field Ultrasound Gel, GF Health Products Inc., Atlanta, Georgia, USA) or petroleum jelly. To assist in preventing current passing from the RF radiative surface to the subject being treated, it is generally preferred that such impedance matching material be non-conductive, for example, petroleum jelly.

The method according to the teachings herein may be implemented using any suitable device. That said, in some embodiments it is preferred to implement the method using a device in accordance with the teachings herein.

Device suitable for the treatment of material through a surface

According to an aspect of some embodiments of the teachings herein there is provided a device suitable for treatment of a volume of material, especially of biological tissue, with energy through a surface, the device comprising:

an ultrasound transducer functionally associated with a sonotrode having an acoustic radiative surface, the ultrasound transducer configured, when activated, to generate acoustic waves that are directed by the acoustic radiative surface into the volume of material through a first portion of a surface with which the acoustic radiative surface is coupled to convey an effective amount of acoustic energy into the volume of material; and

an RF (radio-frequency) applicator having an RF radiative surface, which RF applicator is functionally associable with an RF energy source, the RF applicator configured to direct RF waves, generated by an activated RF energy source functionally-associated with

the RF applicator, to the RF radiative surface to form a unipolar RF field, the unipolar RF field passing through a second portion of the surface with which the RF radiative surface is coupled to deposit an effective amount of thermal energy in the volume of material,, primarily by dielectric heating,

- 5 wherein the device is configured for concurrent depositing of the effective amount of thermal energy and conveying of the effective amount of acoustic energy into the volume of material.

Activation of the ultrasound transducer to generate acoustic waves is as known in the art, typically by providing an appropriately modulated electronic signal from an ultrasound power source to the ultrasound transducer.

- 10 In some embodiments, the surface is a skin surface (especially mammalian skin surface) and the material is hypodermis, especially subcutaneous fat. In such embodiments, the conveying of acoustic energy and the depositing of the thermal energy is through the skin. In such embodiments, the device is configured for the treatment of subcutaneous fat. In some such embodiments, the concurrent depositing of an effective amount of thermal energy (that
15 heats the volume of hypodermis) and conveying of the effective amount acoustic energy (that causes mechanical stress on adipocytes in the volume of hypodermis) is sufficient to initiate a process leading to a reduction of the amount of subcutaneous fat in the volume of hypodermis, in some embodiments more effectively than either when applied alone, for example in accordance with the method of treatment of subcutaneous fat according to the
20 teachings herein.

In some embodiments, the sonotrode and the RF applicator are configured so that the volume of material (e.g., hypodermis) is of between 7 cm^3 and 56 cm^3 .

Shared radiative surface

- 25 As discussed with reference to the method of treatment in accordance with the teachings herein, in some embodiments a radiative surface at least partially shared between the sonotrode and the RF applicator increases the overlap of the volume of material to which an effective amount of acoustic energy is conveyed and the volume of material in which an effective amount of thermal energy is deposited. Accordingly, in some embodiments, at least
30 a portion of the acoustic radiative surface constitutes at least a portion of the RF radiative surface. In some such embodiments, during use of the device the first portion of the (skin) surface through which the acoustic energy is conveyed and the second portion of the (skin) surface through which the thermal energy is deposited at least partially overlap.

In some such embodiments, at least a portion of the acoustic radiative surface constitutes the RF radiative surface. In some such embodiments, during use of the device the second portion of the (skin) surface through which the thermal energy is deposited is a part of the first portion of the (skin) surface through which the acoustic energy is conveyed.

5 In some such embodiments, at least a portion of the RF radiative surface constitutes the acoustic radiative surface. In some such embodiments, during use of the device the first portion of the (skin) surface through which the acoustic energy is conveyed is a part of the second portion of the (skin) surface through which the thermal energy is deposited.

10 In some such embodiments, the acoustic radiative surface constitutes the RF radiative surface. In some such embodiments, during use of the device the first portion of the (skin) surface through which the acoustic energy is conveyed is substantially the same as the second portion of the (skin) surface through which the thermal energy is deposited.

In some such embodiments, such a feature is implemented by using a component that functions as both the sonotrode and as the RF applicator of the device, including parts, subcomponents and assemblies that are bifunctional, serving a function as a part of the sonotrode and a function as part of the RF applicator. Some such embodiments allow simple and convenient use, for implementing embodiments of the teachings herein, but also for treatment exclusively by conveying acoustic energy or depositing thermal energy. Accordingly, in some embodiments of the device as described herein, the sonotrode and the RF applicator are the same component.

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Rigid RF applicator

Some RF applicators known in the art are flexible components unsuitable for use as a sonotrode (e.g., a printed circuit board such as described in US 7,452,358) due to the inefficiency of flexible components for conveying acoustic energy. In contrast, in some embodiments of a device herein, and particularly embodiments where at least a portion of the acoustic radiative surface constitutes at least a portion of the RF radiative surface, the RF applicator is sufficiently rigid for conveying the effective amount of acoustic energy. In some such embodiments, the RF applicator is substantially a solid rigid mass of electrically-conductive material.

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Concurrent activation of ultrasound transducer and RF energy source

In some embodiments, the configuration for concurrent depositing of an effective amount of thermal energy and conveying of an effective amount of acoustic energy includes

configuration for concurrent activation of the ultrasound transducer and of a functionally-associated RF energy source.

In some embodiments of a device as described herein, the device is configured so that concurrent activation of the ultrasound transducer and of an RF energy source functionally-associated with the RF applicator is mandatory. In such embodiments, activation of a functionally-associated RF energy source is always concurrent with activation of the ultrasound transducer.

In some embodiments of a device described herein, the device is configured so that concurrent activation of the ultrasound transducer and of an RF energy source functionally-associated with the RF applicator is optional. Typically, such embodiments allow a user to select operation of the device in a “concurrent mode” where the ultrasound transducer and a functionally-associated RF energy source are operated concurrently, and at least one other mode. During operation in “concurrent mode”, the ultrasound transducer and a functionally-associated RF energy source are concurrently activated, for example, allowing conveying of acoustic energy with concurrent depositing of thermal energy, for example in accordance with the method of treatment according to the teachings herein.

In some such embodiments of a device where concurrent activation is optional, the device is configured to allow at least two modes of operation: a mode of “acoustic only” where the ultrasound transducer is activated alone (for example, allowing conveying of acoustic energy without concurrent depositing of thermal energy, for example as described in US 2011/0213279) and a “concurrent mode”.

In some such embodiments of a device where concurrent activation is optional, the device is configured to allow at least two modes of operation: a mode of “RF only” where a functionally-associated RF energy source is activated alone (for example, allowing depositing of thermal energy alone without concurrent conveying of acoustic energy, for example as described in US 7,630,774) and a “concurrent mode”

In some such embodiments of a device where concurrent activation is optional, the device is configured to allow at least three modes of operation: an “ultrasonic only” mode, an “RF only” mode and a “concurrent mode”.

In some embodiments, the device is configured so that the concurrent activation of the ultrasound transducer and of an RF energy source functionally-associated with the RF applicator is at least optionally simultaneous activation, allowing simultaneous conveying of acoustic energy and depositing of thermal energy. In some embodiments, such simultaneous

activation is mandatory. In some embodiments, such simultaneous activation is optional, e.g., selected by a user of the device.

In some embodiments, the ultrasound transducer is configured for continuous activation during a period of time (typically at least 10 seconds, more typically at least 5 minutes or for a length of time limited by the user) for continuous conveying of acoustic energy during the period of time; and a functionally-associated RF energy source is configured for discontinuous activation (including at regular or irregular intervals, periodic, non-periodic) during the period of time, for discontinuous depositing of thermal energy. In some such embodiments, discontinuous activation of a functionally-associated RF energy source is periodic activation, in some embodiments at a rate not slower than 0.2 Hz.

In some embodiments, the device is configured so that concurrent activation of the ultrasound transducer and of a functionally-associated RF energy source is at least optionally alternating activation, allowing alternatingly conveying of acoustic energy and depositing of thermal energy during a period of time, in some embodiments the alternating activation is at a rate not slower than 0.2 Hz.

Cooling assembly

As discussed with reference to the method of treatment in accordance with the teachings herein, depositing thermal energy potentially leads to undesirable side-effects, such as excessive heating and even burning of a surface coupled with the RF radiative surface, for example, burning of a skin surface when a functionally-associated RF energy source is activated. To reduce or avoid the incidence of such undesirable side-effects when the device is used and the RF energy source is activated, in some embodiments the device is configured to actively cool a portion of a surface during treatment of a volume of material with the device.

To this end, in some embodiments, a device further comprises a cooling assembly configured, when activated, to cool at least one of the acoustic radiative surface and the RF radiative surface. Since undesirable side effects (such as skin-burning) typically occur in proximity to the RF radiative surface, in some embodiments cooling of one or both of the radiative surfaces allows cooling of a potentially affected surface.

In some embodiments, a device further comprises cooling-fluid channels in thermal communication with at least one of the acoustic radiative surface and the RF radiative surface. In some such embodiments, the cooling-fluid channels are in thermal communication with at least one of the sonotrode and the RF applicator.

During use of the device, such cooling-fluid channels can be functionally associated with an appropriately configured cooling device or cooling assembly that drives a cooling fluid through the cooling-fluid channels, thereby cooling at least one of the acoustic radiative surface and the RF radiative surface. In some embodiments, the device further comprises a cooling assembly functionally associated with the cooling-fluid channels configured, when activated, to drive a cooling fluid through the cooling-fluid channels, thereby cooling at least one of the acoustic radiative surface and the RF radiative surface.

In some embodiments, a cooling assembly is activatable during at least one of activation of the ultrasound transducer and of an RF energy source functionally-associated with the RF applicator.

In some embodiments, in addition to including a cooling assembly to cool a radiative surface or in addition to being configured for use with a cooling assembly to cool a radiative surface, a device includes an RF energy source or is configured to be functionally-associated with an RF energy source configured in accordance with the teachings of US 7,630,774. When such an RF energy source is activated to generate RF waves to implement the teachings herein, such an RF energy source allows the surface to remain at a substantially lower temperature than deeper layers of the volume of material, reducing the incidence of undesirable side-effects.

In some embodiments, a device as described herein is devoid of a cooling assembly and/or is not configured to be functionally associated with a cooling assembly but includes an RF energy source or is configured to be functionally-associated with an RF energy source configured in accordance with the teachings of US 7,630,774 allowing a surface to remain at a substantially lower temperature than deeper layers of the volume of tissue when the RF energy source is activated.

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Acoustic waves

The ultrasound transducer, the sonotrode and the acoustic radiative surface are configured to generate and direct acoustic waves of any suitable characteristics (frequencies, energy and modes of use) that are effective for an intended use, for example for treatment of subcutaneous fat, for example as disclosed in US 2011/0213279. The ultrasound transducer is any suitable ultrasound transducer, for example similar to that disclosed in US 2011/0213279. The sonotrode is any suitable sonotrode, for example similar to that disclosed in US 2011/0213279. The acoustic radiative surface is any suitable acoustic radiative surface, for example similar to that disclosed in US 2011/0213279.

In some embodiments, the ultrasound transducer, the sonotrode and the acoustic radiative surface are together configured so that the acoustic energy is conveyed by longitudinal acoustic waves, for example as disclosed in US 2011/0213279.

5 In some embodiments, the ultrasound transducer, the sonotrode and the acoustic radiative surface are together configured so that acoustic energy is conveyed by transverse ultrasonic mechanical waves, for example as disclosed in US 2011/0213279.

In some embodiments, the ultrasound transducer, the sonotrode and the acoustic radiative surface are together configured so that acoustic energy is conveyed by both transverse and longitudinal ultrasonic mechanical waves, for example as disclosed in US
10 2011/0213279.

In some embodiments, the ultrasound transducer, the sonotrode and the acoustic radiative surface are together configured so that acoustic energy is alternatingly conveyed by transverse and longitudinal ultrasonic mechanical waves, for example as disclosed in US
15 2011/0213279.

RF Waves

The RF applicator is configured to direct RF waves generated by a functionally-associated RF energy source and the RF radiative surface is configured to form a unipolar RF field therefrom, the RF waves having any suitable characteristics (frequency, energy, modes
20 of use) that are effective for the intended use in accordance with the teachings herein, for example for treatment of subcutaneous fat as disclosed in US 7,630,774. An RF energy source that is a component of the device or that the device is configured to be functionally-associated with is any suitable RF energy source, for example similar to that disclosed in US 7,630,774. The RF applicator is any suitable RF applicator, for example similar to that
25 disclosed in US 7,630,774. The RF radiative surface is any suitable RF radiative surface, for example similar to that disclosed in US 7,630,774.

That said and as discussed with reference to the method according to the teachings herein, since the preferred mode of depositing thermal energy is dielectric heating with a unipolar RF field, in some embodiments the RF applicator is configured to direct RF waves
30 and the RF radiative surface is configured to form a unipolar RF field therefrom having a frequency of not less than 2 MHz, not less than 4 MHz and in some embodiments not less than 10 MHz, and in typical preferred embodiments, between 10 MHz and 100 MHz.

In some embodiments the configuration of the RF applicator and of the RF radiative surface is for RF waves having a frequency in an Industrial, Scientific and Medical frequency

band, e.g., selected from the group consisting of $13.560\text{MHz} \pm 7\text{kHz}$, $27.120\text{ MHz} \pm 163\text{ kHz}$, $40.68\text{ MHz} \pm 20\text{ kHz}$, $2.45\text{ GHz} \pm 50\text{ MHz}$, $5.800\text{ GHz} \pm 75\text{ MHz}$, $24.125\text{ GHz} \pm 125\text{ MHz}$, $6.780\text{ MHz} \pm 15\text{kHz}$, $61.25\text{ GHz} \pm 250\text{ MHz}$, $122.5\text{ GHz} \pm 500\text{ MHz}$, $245\text{ GHz} \pm 1\text{ GHz}$, $433.92\text{ MHz} \pm 870$ and $915\text{ MHz} \pm 13\text{ MHz}$.

5 In some embodiments the configuration of the RF applicator and of the RF radiative surface is for RF waves having a frequency of $13.560\text{ MHz} \pm 7\text{ kHz}$, $27.120\text{ MHz} \pm 163\text{ kHz}$, $915\text{ MHz} \pm 13\text{ MHz}$, but most especially $40.68\text{ MHz} \pm 20\text{ kHz}$.

In some embodiments, the device further comprises an RF energy source functionally associated with the RF applicator configured, when activated, to generate RF waves sufficient
10 so that the unipolar RF field formed at the RF radiative surface is sufficient to deposit an effective amount of thermal energy into the volume of material. By "effective amount" is meant an amount sufficient to cause or initiate a desired effect in the volume of material. Such an RF energy source is configured to generate RF waves of any suitable RF frequency. That said, as discussed with reference to the method according to the teachings herein, since
15 the preferred mode of depositing thermal energy is dielectric heating with a unipolar RF field, in some embodiments it is preferred that the RF energy source is configured to generate RF waves having a frequency of not less than 2 MHz, not less than 4 MHz and in some embodiments not less than 10 MHz, and in typical preferred embodiments, between 10 MHz and 100 MHz, especially $13.560\text{ MHz} \pm 7\text{ kHz}$, $27.120\text{ MHz} \pm 163\text{ kHz}$, $915\text{ MHz} \pm 13$
20 MHz, but most especially $40.68\text{ MHz} \pm 20\text{ kHz}$.

In some embodiments, the surface is a skin surface, the material is hypodermis and the RF applicator and the RF radiative surface are together configured so that a formed unipolar RF field deposits an effective amount of thermal energy sufficient to heat the volume of hypodermis. In some such embodiments, the effective amount of thermal energy
25 deposited is sufficient to raise (and in some embodiments maintain) the temperature of a volume of hypodermis to a temperature of between 42°C and 48°C , or even to a temperature of between 42°C and 46°C .

As noted above any suitable ultrasound transducer, sonotrode and acoustic radiative surface may be used in implementing a device as disclosed herein. Further, as also noted
30 above any suitable RF energy source, RF applicator and RF radiative surface may be used in implementing a device as disclosed herein.

That said and also as noted above, in some embodiments, at least a portion of the acoustic radiative surface constitutes at least a portion and even all of the RF radiative surface, and in some embodiments, the ultrasound radiative surface constitutes the RF

radiative surface. In some such embodiments, the sonotrode and the RF applicator are the same component.

In the art (for example, in US 2011/0213279), it is known that to effectively convey acoustic energy into a material, a sonotrode is preferably a solid rigid component, having an acoustic impedance as close as possible to that of the material. For example to treat biological tissue having an acoustic impedance of 1.3 - 2.0 MRayls ($\text{kg} / (\text{sm}^2 \times 10^6)$), a sonotrode is typically glass or porcelain (~13 MRayls) or a metal having a low acoustic impedance like aluminum and aluminum alloys (~17 MRayls). It is also known to coat the acoustic radiative surface of a sonotrode with an acoustic matching layer, a layer of a sufficient thickness of a material having an acoustic impedance between that of the sonotrode and the material into which the acoustic energy is conveyed. When the material is biological tissue, suitable acoustic matching layers are layers of PVDF (polyvinylidene fluoride, 4.2 MRayl) or PTFE (polytetrafluoroethylene, 3 MRayl), typically 1 to 50 micrometers thick, preferably 5 to 20 micrometers thick.

The Inventors have recognized that although RF applicators known in the art are typically flexible components unsuitable for use as a sonotrode (e.g., a printed circuit board such as described in US 7,452,358), it is possible to use a component that is substantially a solid rigid (that is sufficiently rigid for conveying acoustic energy) mass of electrically conductive material as both an RF applicator and as a sonotrode: the electrical conductivity of the material renders such a combined component suitable for use as a waveguide to guide RF waves and the rigidity of the material renders such a combined component suitable for conveying acoustic energy.

Thus, in some embodiments of a device in accordance with the teachings herein, an RF applicator is substantially a solid rigid mass of electrically-conductive material. In some such embodiments, the RF applicator is a single integrally-formed component. Typical such materials include aluminum (17.3 MRayls), titanium (27 MRayls), silver (38 MRayls), copper (44.6 MRayls), gold (63.8 MRayls) and alloys thereof.

Particularly, in US 2011/0213279 is disclosed a sonotrode which description, details, and modes of use as if fully set-forth herein. The Inventors have recognized that in some embodiments, a similar such sonotrode can be appropriately modified for use also as an RF applicator in accordance with the teachings herein. In some such embodiments, the sonotrode is configured (inter alia, in terms of shape and dimensions) to be suitable for conveying both longitudinal and transverse acoustic energy, as described in US 2011/0213279.

As noted above, in some embodiments a device as described herein comprises or is functionally associated with a cooling assembly configured to cool, when activated, at least one of the acoustic radiative surface and the RF radiative surface, for example to reduce the incidence of undesired side-effects such as burning of a surface such as of skin. In some such
5 embodiments, the cooling assembly comprises cooling-fluid channels in thermal communication with at least one of the sonotrode and the RF applicator. For example, in some embodiments, especially when the RF applicator is a solid rigid mass of conductive material, the cooling-fluid channels are in thermal communication with a portion of the RF applicator. Since the RF applicator is of a solid electrically-conductive material, thermal
10 conduction through the RF applicator is efficient. In such embodiments, when the cooling assembly is activated, cooling fluid (e.g., a gas or liquid, typically a liquid such as water or an aqueous solution) flows through the cooling-fluid channels, cooling the portion of the RF applicator, and by conduction through the solid mass, also the RF radiative surface.

In some embodiments, the cooling-fluid channels pass through a component separate
15 from the RF applicator that contacts a portion of the RF applicator and are thereby in thermal communication with the RF applicator and the RF radiative surface.

In some embodiments, the cooling-fluid channels pass through bulk of the RF applicator and are thereby in thermal communication with the RF applicator and the RF radiative surface. In some such embodiments, it is important that the dimensions and location
20 of the cooling-fluid channels be such as to not interfere with the functioning of the RF applicator as a sonotrode, e.g., by causing internal reflection of acoustic waves or by substantially reducing the structural integrity of the RF applicator.

It is known that an RF radiative surface of an RF applicator may optionally comprise a layer of a dielectric material as an electrical insulator to prevent conduction of current
25 therethrough, into biological tissue being treated, as taught in US 7,630,774. As noted above, it is also known that an acoustic radiative surface of a sonotrode comprises an acoustic matching layer to increase the efficiency of conveying of acoustic energy from the sonotrode into the biological tissue. The Inventors have recognized that some acoustic matching layers are dielectric and can therefore also serve as an electrical insulator to prevent conduction of
30 current therethrough. Accordingly, in some embodiments (especially where at least a portion of the acoustic radiative surface constitutes at least a portion of the RF radiative surface) a portion of the acoustic radiative surface constituting at least a portion of the RF radiative surface comprises a layer of a dielectric material, the layer having a thickness sufficient to substantially prevent conduction of current therethrough when a functionally-associated RF

energy source is activated and the layer also suitable for functioning as an acoustic matching layer when the ultrasound transducer is activated. Suitable materials from which such a layer is fashioned include PVDF (polyvinylidene fluoride, 4.2 MRayl) and PTFE (polytetrafluorethylene, 3 MRayl), typically 1 to 50 micrometers thick, preferably 5 to 20 micrometers thick.

In some embodiments, the sonotrode and the RF applicator are the same component fashioned of a solid rigid mass of aluminum or aluminum alloy, similar to the solid aluminum sonotrode disclosed in US 2011/0213279. The electrical conductivity of aluminum and alloys thereof is relatively low (compared to silver, gold and copper), but despite this has been surprisingly found to be sufficient for acting as a waveguide to implement the teachings herein. The acoustic impedance of aluminum and alloys thereof (~17.3 MRayls) is relatively high compared to that of biological tissue, but is significantly lower than that of other materials having a high electrical conductivity (e.g., silver, gold and copper). An additional advantage of aluminum and alloys thereof is the layer of aluminum oxide (alumina, Al_2O_3) that naturally forms on a surface thereof. The aluminum oxide forms a natural dielectric layer that functions as an electrical insulator to prevent conduction of current therethrough, into biological tissue being treated and burning of the biological tissue. Aluminum oxide has an exceptionally high acoustic impedance (40.6 MRayls) but it has been found that the aluminum oxide layer naturally forming on a solid rigid mass of aluminum such as a sonotrode as described herein is typically thin enough (about 4 nm) to not substantially interfere with the conveying of acoustic energy from an ultrasound transducer to a volume of hypodermis. That said, in some embodiments a thicker aluminum oxide layer is applied (e.g., by anodization or by sputtering) to reduce the chance of burning of tissue and/or conduction of current therethrough. Typically, such a thicker aluminum oxide layer is not more than 75 micrometers thick, not more than 50 micrometers thick and even not more than 40 micrometers thick. In some such embodiments, such a thicker aluminum oxide layer is between 5 micrometers and 15 micrometers (e.g., 10 micrometers) thick. It has been surprisingly been found that such a thick layer of aluminum oxide does not substantially adversely affect the ability of a radiative surface to direct acoustic waves through a skin surface when the RF applicator functions as a sonotrode in accordance with the teachings herein.

In some such embodiments, the radiative surface is coated with an acoustic matching layer (e.g., PVDF or PTFE) on the aluminum oxide layer. Such double layer coating improves the acoustic coupling of the acoustic radiative surface and tissue and also assists in

preventing conduction of electrical current therethrough and/or burning of tissue, especially if the aluminum oxide layer is cracked or otherwise damaged. In such embodiments, the aluminum oxide layer is not more than 75 micrometers thick, not more than 50 micrometers thick, not more than 40 micrometers thick, and even between 5 micrometers and 15 micrometers (e.g., 10 micrometers) while the acoustic matching layer applied to the surface of the aluminum oxide layer (e.g., of PVDF or PTFE) is typically 1 to 50 micrometers thick, preferably 5 to 20 micrometers thick.

First embodiment of a device according to the teachings herein

10 An embodiment of a device for the treatment of a volume of material with energy through a surface, specifically for treatment of subcutaneous fat as described herein, device **10**, is schematically depicted in Figures 1A-1F. In Figure 1A, device **10** is depicted fully assembled, viewed in perspective from a distal end **12**. In Figure 1B, device **10** is depicted fully assembled, viewed in perspective from a proximal end **14**. In Figure 1C, device **10** is depicted with some components removed to show details of construction, viewed from the side. In Figures 1D, 1E and 1F, device **10** is depicted with some components removed to show details of construction, viewed in perspective.

Device **10** is a probe configured for concurrently depositing an effective amount of thermal energy into a volume of hypodermis with a unipolar RF field through a skin surface and for conveying an effective amount of acoustic energy into the volume of hypodermis through a skin surface in accordance with embodiments of the method according to the teachings herein. Specifically, the concurrent depositing of the effective amount of thermal energy and of the effective amount of acoustic energy is sufficient to initiate a process leading to a reduction of the amount of fat in the volume of hypodermis.

25 Device **10** comprises a rigid stacked ultrasound transducer **16** with a distally-located sonotrode **18** having an acoustic radiative surface **20** and a cooling assembly made up of two independently-operable portions, distal cooling assembly **22a** and proximal cooling assembly **22b**. A cooling-fluid channel of distal cooling assembly **22a** is in thermal communication with sonotrode **18** and, through the bulk of sonotrode **18**, acoustic radiative surface **20**.

30 Sonotrode **18** also functions as an RF applicator so that in device **10** the sonotrode and the RF applicator are the same component and so that at least a portion of acoustic radiative surface **20** constitutes at least a portion of the RF radiative surface, specifically, acoustic radiative surface **20** constitutes the RF radiative surface of the RF applicator of device **10**.

Sonotrode / RF applicator

Sonotrode / RF applicator **18** is fashioned from a single solid homogenous rigid block of aluminum alloy (Al 7075), substantially as described in US 2011/0213279, allowing functioning both as an RF applicator and to direct acoustic waves through radiative surface
 5 **20**.

Substantially all exposed surfaces of sonotrode/RF applicator **18**, and particularly radiative surface **20** are coated with a native layer of alumina formed by exposure of aluminum metal to atmospheric oxygen. The alumina layer is dielectric and of sufficient thickness to substantially prevent conduction of current through radiative surface **20** when an
 10 RF energy source functionally-associated with sonotrode / RF applicator **18** is activated. The alumina layer is sufficiently thin so as not to substantially impede passage of acoustic waves through radiative surface **20**.

Radiative surface **20** includes a plurality of concentric circular ridges, similar to that described in US 2011/0213279. The diameter of radiative surface **20** is 4 cm, allowing device
 15 **10** to concurrently convey an effective amount of acoustic energy and/or deposit an effective amount of thermal energy to a cylinder of tissue having a diameter of up to about 4 cm and to a depth of up to about 2 cm deep, that is to say a volume of hypodermis of up to about 25 cm³.

20 *Stacked ultrasound transducer*

The components and assembly of stacked ultrasound transducer **16** are clearly depicted in Figures 1, especially Figure 1C and Figure 1D.

In Figure 1D, sonotrode / RF applicator **18** is depicted as transparent, showing central shaft **24** which a distal end **26** thereof is screwed into and thereby secured into a hole in the
 25 proximal end of sonotrode / RF applicator **20**. For clarity, not depicted are the threads on distal end **26** or the counter-threads in the hole in sonotrode / RF applicator **20**.

Intimately contacting and surrounding most of the length of central shaft **24** is electrically insulating sleeve **30** of PTFE (a tube having a wall thickness of 1-2 mm) which distal end contacts a proximal face **32** of sonotrode / RF applicator **20**.

30 At a proximal end **28** of central shaft **24** is a sapphire insulating washer **34** having a larger diameter than insulating sleeve **30**. Insulating washer **34** is partially surrounded by a rubber washer **36**.

A brass nut **38** is screwed over threads (not depicted) on proximal end **28** of central shaft **24** to the extent that brass nut **38** presses insulating washer **34** and insulating sleeve **30** tightly together and against proximal face **32** of sonotrode / RF applicator **20**.

In Figure 1C, the components of device **10** that are stacked along central shaft **24** between sonotrode / RF applicator **18** and insulating washer **34**, and electrically insulated from central shaft **24** are depicted. From proximal to sonotrode / RF applicator **18** in a proximal direction, the components are: a brass sleeve **40** (which distal end cups and is in intimate contact with a proximal end **42** of sonotrode / RF applicator **18**), a sapphire insulator ring **44**, a distal transducer plate **46**, a distal piezoelectric ceramic ring **48**, a central transducer plate **50**, a proximal piezoelectric ceramic ring **52**, a proximal transducer plate **54**, negative contact **56** and a proximal cooling assembly **22b**. The stacked components all have a central hole dimensioned to intimately fit over insulating sleeve **30**, preventing any substantial movement of the components perpendicularly to the axis of central shaft **24**. The thicknesses of the stacked components are such that when device **10** is fully assembled, brass nut **38** presses against insulating washer **34** that presses against a proximal face **58** of proximal cooling assembly **22b** so that the stacked components are all tightly pressed together and against proximal face **32** of sonotrode / RF applicator **18**, preventing any substantial movement of the components.

20 *Cooling Assembly*

As noted above, device **10** comprises a cooling assembly made up of two independently-operable portions, distal cooling assembly **22a** and proximal cooling assembly **22b**.

25 *Distal cooling assembly*

Surrounding a proximal portion **60** of brass sleeve **40** and held in place against a flange **62** of brass sleeve **40** with screws **64** is distal cooling assembly **22a** including a brass distal cooling envelope **66a**. A distal cooling channel is defined by a portion **68** of an outer surface of proximal portion **60** of brass sleeve **40** between two O-rings (not depicted) placed in grooves **70**, the two O-rings, and an inner surface of distal cooling envelope **66a**. The distal cooling channel is in fluid communication with a distal cooling fluid inlet **72a** and a distal cooling fluid outlet **74a**. Cooling fluid entering through cooling fluid inlet **72a** is forced through the distal cooling channel to contact portion **68** of the outer surface of proximal

portion **60** of brass sleeve **40** to cool brass sleeve **40** and, by thermal conduction, sonotrode / RF applicator **18** and radiative surface **20**.

Proximal cooling assembly

5 Proximal cooling assembly **22b** is stacked along central shaft **24** surrounding insulating sleeve **30**. Proximal cooling assembly **22b** includes a hollow proximal cooling envelope **66b** that defines a proximal cooling channel in fluid communication with a proximal cooling fluid inlet **72b** and a proximal cooling fluid outlet **74b**. Cooling fluid entering through cooling fluid inlet **72b** is forced through the proximal cooling channel to
10 cool the walls of proximal cooling envelope **66b**, and by thermal conduction, negative contact **56**, proximal transducer plate **54**, proximal piezoelectric ceramic ring **52**, central transducer plate **50**, distal piezoelectric ceramic ring **48** and distal transducer plate **54**.

Coaxial cable and coil

15 A coaxial cable **76** and a copper coil **78** provide functional association of device **10** with an RF energy source. Coaxial cable **76** is any (commercially-available) coaxial cable able to direct RF waves for operating device **10** as described above. Copper coil **78** is a coil selected to function as a high-impedance inductor for RF electrical currents (e.g., 40 MHz) but as a conductor for lower frequency electrical currents (e.g., less than 200 kHz)

20 The outer conductive shield of coaxial cable **76** is in direct electrical contact with negative contact **56** so that negative contact **56** and proximal transducer plate **54** are ground for an RF current from coaxial cable **76**. The outer conductive shield of coaxial cable **76** is in electrical contact with distal cooling envelope **66a**, brass sleeve **40** and sonotrode / RF applicator **18** through coil **78**.

25 The inner conductive core of coaxial cable **76** is in direct electrical contact with distal cooling envelope **66a**, brass sleeve **40** and sonotrode / RF applicator **18** to direct RF waves from an RF energy source to sonotrode / RF applicator **18**.

As is clear to one skilled in the art, the stacked construction of ultrasound transducer **16** constitutes a capacitor, most significantly across sapphire insulator ring **44** between distal
30 transducer plate **46** and the proximal face of brass sleeve **40**. Such a capacitor absorbs power from RF waves, potentially preventing conduction of a sufficiently powerful RF waves to sonotrode / RF applicator **18**. To avoid such an effect, copper coil **78** acts as an inductor at radiofrequencies (e.g., 40 MHz) located in parallel to the capacitor, lowering the impedance of the circuit and thus preventing the capacitor from absorbing energy from RF waves. For

lower frequencies, e.g., less than 200 kHz such as ultrasound, coil **78** acts as a short circuit between sonotrode / RF applicator **18** and negative contact **56**.

Operation of device 10

5 As device **10** is substantially a probe, for use device **10** must be functionally associated with other devices to function: an RF energy source to generate and provide RF waves through coaxial cable **24**, an ultrasound power source to generate and provide an appropriately-modulated alternating current to plates **46**, **50** and **54** of ultrasound transducer **16** and a cooling fluid pump to generate, drive and recycle cooling fluid through cooling-fluid
10 channels of cooling assembly **22a** and **22b**.

To generate and convey acoustic energy through radiative surface **20**, an ultrasound power source is functionally associated with ultrasound transducer **16**, by electrically connecting a positive lead of the ultrasound power source to central transducer plate **50** and electrically connecting a ground lead of the ultrasound power source to distal transducer plate
15 **48** and to proximal transducer plate **52**. As known in the art of "sandwich type" ultrasound transducers, ultrasound transducer **16** is activated when the ultrasound power source generates an appropriately-modulated current alternating at a desired frequency, typically of between 1 kV and 1.5 kV alternating at between 100 kHz and 160 kHz, generating an alternating electrical field between the pairs of transducer plates **46** / **50** and **50** / **54**.
20 Piezoelectric ceramic rings **48** and **52** located in the alternating electrical field between the pairs of transducer plates axially expand and relax at the frequency of the electric field, producing ultrasonic vibrations that are transmitted through the rigid structure of ultrasound transducer **16**, including radiative surface **20** of sonotrode / RF applicator **18** as acoustic waves. If radiative surface **20** is acoustically coupled with a surface of a material such as a
25 skin surface, radiative surface **20** directs the acoustic waves into the volume of material through the surface to convey acoustic energy into the volume of the material. Depending on the frequency of the current from the ultrasound power source, sonotrode / RF applicator **18** directs longitudinal (~100 kHz) or transverse (~160 kHz) acoustic waves through radiative surface **20**, as described in US 2011/0213279. .

30 To deposit thermal energy in the volume of material through radiative surface **20**, an RF energy source is functionally associated with sonotrode / RF applicator **18** through coaxial cable **76**. The RF energy source is activated to generate RF waves (e.g., 40.68 MHz $\pm$ 20 kHz) that are directed by coaxial cable **76** through distal cooling envelope **66a**, brass sleeve **40** to sonotrode / RF applicator **18**. Sonotrode / RF applicator **18** directs the RF waves

to radiative surface **20** where a unipolar RF field having a frequency of the RF current is formed. The unipolar RF field deposits an effective amount of thermal energy in the volume of material by dielectric heating.

The ultrasound power source and the RF energy source can activated separately or
5 concurrently (including simultaneously), allowing both separate and concurrent (including simultaneous) conveying of acoustic energy and depositing of thermal energy in a volume of material through radiative surface **20**.

Second embodiment of a device according to the teachings herein

10 An additional embodiment of a device for the treatment of a volume of material with energy through a surface, specifically for the treatment of subcutaneous fat as described herein, device **80**, is schematically depicted in Figure 2 during use for treatment of a volume **82** of tissue including subcutaneous fat **84** through a skin surface **86**. It is important to note, particularly with regard to Figure 2, that some objects are not depicted to scale for clarity.

15 Device **80** comprises a probe **88**, substantially identical to device **10** described with reference to Figures 1, and additionally comprises a controller **90**, an RF energy source **92** (e.g., such as described in US 7,630,774) functionally associated with a sonotrode/RF applicator **18** of probe **88** through controller **90** and coaxial cable **76** and an ultrasound power source **94** (e.g., such as described in US 2011/0213279) functionally associated with an
20 ultrasound transducer **16** through controller **90** and leads **96**.

Device **80** also comprises cooling fluid pump **98**, that is functionally associated with the cooling fluid channels of the cooling assemblies of probe **88** through the cooling fluid and outlets, cooling fluid pump **98** configured to produce and drive water chilled to between 0° and 20°C as a cooling fluid through the cooling-fluid channels via conduits **100a** and **100b**,
25 standard flexible cooling-fluid conduits known in the art.

In Figure 2, device **80** is depicted where a radiative surface **20** of a sonotrode/RF applicator **18** of probe **88** is coupled (by direct contact after application of petroleum jelly) to a skin surface **86** of a human subject.

For use in treating subcutaneous fat, a user activates controller **90** and selects a mode
30 of operation.

The user can select a first "ultrasonic only" mode of use where only the ultrasound transducer of device **80** is activated (and not RF energy source **92**) for treatment of volume of tissue **82** with acoustic energy alone, as known in the art, for example as described in US 2011/0213279. As known in the art, the user selects the various acoustic energy parameters

(intensity, frequency, transverse and/or longitudinal waves) through controller **90**. Controller **90** activates ultrasound power source **94** to provide an appropriately-modulated electronic signal (in accordance to the user-selected parameters) to the ultrasound transducer, thereby activating the ultrasound transducer to convey an effective amount of acoustic energy into
5 volume **82** of tissue through skin surface **86**, leading to a desired effect.

Alternatively, the user can select a second "RF only" mode of use where only RF energy source **92** is activated (and not the ultrasound transducer) for treatment of with thermal energy alone, as known in the art, for example as described in US 7,630,774. As known in the art, the user selects the various RF parameters (e.g., intensity, frequency)
10 through controller **90**. Controller **90** activates RF energy source **92** to provide appropriately-modulated RF waves (in accordance to the user-selected parameters) that are directed by sonotrode / RF applicator **18** to radiative surface **20** to form a unipolar RF field at radiative surface **20** that deposits an effective amount of thermal energy through skin surface **86** to volume of tissue **82**. Consequently and as known in the art, the temperature of the
15 subcutaneous fat in volume **82** of tissue rises (e.g., temperature of between 42°C and 48°C), leading to a desired effect.

Alternatively, the user can select a third "concurrent" mode of use where RF energy source **92** is activated (substantially as described above) concurrently with activation of the ultrasound transducer (substantially as described above). By concurrent activation is meant in
20 accordance with any of the embodiments of the method of treatment as described above (including simultaneous and alternating activation). Due to the fact that ultrasound radiative surface **20** constitutes the RF radiative surface, the intersection of the volume of tissue in which the thermal energy is deposited and the volume of tissue into which acoustic energy is conveyed, and consequently the volume **82** to which an effective amount of thermal energy is
25 deposited concurrently with conveying of an effective amount of acoustic energy is maximal, depending in the user-defined settings, up to 25 cm³.

As is known in the art, the user can move radiative surface **20** to portions of skin surface of the treated subject different from surface **86** to treat volumes of hypodermis different from volume **82**.

30 Independently of controller **90**, at any time and during operation of device **80** in any mode, a user optionally also activates cooling fluid pump **98** and selects a cooling fluid temperature (typically between 15° and 20°C). Cooling fluid pump **98** operates, chilling a cool fluid (water) and driving the chilled cooling fluid through conduits **100a** and **100b**.

Cooling fluid pump **98** drives the chilled cooling fluid through conduit **100a** into the distal cooling channel of probe **88**. As the distal cooling fluid channel is in thermal communication therewith, the cooling fluid cools sonotrode/RF applicator **18**, radiative surface **20** and thereby skin surface **86**, numbing the skin and reducing the chance of
5 undesirable side-effects such as burning of the skin surface.

In the embodiments described above with reference to the figures, radiative surface **20** of sonotrode / RF applicator **18** includes a plurality of concentric circular ridges as described in US 2011/0213279. In some, non-depicted, related embodiments, the radiative surface
10 includes other features, for example as described in US 2011/0213279, such as multiple discontinuous surfaces, plurality of protrusions, plurality of vertical ridges.

In the embodiments described above with reference to the figures, sonotrode / RF applicator **18** has a shape and dimensions allowing delivery of longitudinal ultrasonic waves at ~100 kHz and delivery of transverse ultrasonic waves at ~160 kHz through radiative
15 surface **20**, as described in US 2011/0213279. In some embodiments, a sonotrode / RF applicator has a different shape and/or dimensions for delivering different frequencies of longitudinal and/or transverse ultrasonic waves.

In the embodiments described above with reference to the figures, radiative surface **20** of sonotrode / RF applicator **18** is coated with a native (about 4 nm thick) electrically-
20 insulating layer of dielectric alumina. In some embodiments, a radiative surface of an RF applicator is coated with a thicker electrically-insulating layer, for example, not more than 50 micrometers, not more than 40 micrometers, more typically between 5 micrometers and 15 micrometers (e.g., 10 micrometers) thick layer of alumina (e.g. applied by anodization or sputtering). It has been surprisingly been found that such thick layers of alumina do not
25 substantially adversely affect the ability of a radiative surface **20** to direct acoustic waves through a skin surface when the RF applicator functions as a sonotrode in accordance with the teachings herein.

In some embodiments, a radiative surface **20** is coated (additionally to an alumina layer) with a second layer (e.g., of PTFE or PVDA) that functions as an acoustic matching
30 layer when an ultrasound transducer **16** is activated, and in some embodiments the second layer functions also as an additional layer to prevent conduction of current through radiative surface **20** when a functionally-associated RF energy source such as **92** is activated.

In some embodiments, a radiative surface **20** is coated (instead of the alumina layer) with a layer (e.g., of PTFE or PVDA) that functions both as as an acoustic matching layer

when an ultrasound transducer **16** is activated and as a dielectric layer to prevent conduction of current through radiative surface **20** when a functionally-associated RF energy source such as **92** is activated.

In the embodiments described above with reference to the figures, coil **78** functions as an inductor to prevent loss of energy from RF waves generated by an RF energy source. In some embodiments, other types of inductors are used instead.

In the embodiments described above with reference to the figures, the outer conductive shield of coaxial cable **76** is in direct electrical contact with negative contact **56** so that negative contact **56** and proximal transducer plate **54** are ground for an RF current from coaxial cable **76**. In some embodiments, the outer conductive shield of coaxial cable **76** is in direct electrical contact (alternately or additionally) with other components of a transducer, e.g., a central transducer plate such as **50** or a distal transducer plate such as **46**.

In the embodiments described above with reference to the figures, devices **10** and **80**, and especially the respective radiative surfaces **20** of sonotrodes / RF applicators **18** are configured to concurrently convey an effective amount of acoustic energy and deposit an effective amount of thermal energy to a cylinder of tissue having a volume of up to 25 cm³. In some embodiments, the maximal size of such a volume of tissue is greater or lesser, in some embodiment up to 56 cm³.

In the embodiment described above with reference to Figure 2, controller **90** of device **80** is configured to allow a user to use device **80** in three modes: activation of the ultrasound transducer for acoustic energy treatment alone, activation of RF energy source **92** for thermal energy treatment alone, and concurrent activation for concurrent treatment.

In some embodiments, a device is configured for mandatory concurrent activation of an ultrasound transducer and of an RF energy source.

In some embodiments, such a device is configured to allow a user to use the device in two modes: activation of the ultrasound transducer for conveying acoustic energy only or concurrent activation of the RF energy source for thermal energy deposition with activation of the ultrasound transducer for conveying acoustic energy.

In some embodiments, such a device is configured to allow a user to use the device in two modes: activation of the RF energy source for RF energy treatment only or concurrent activation of the RF energy source for thermal energy deposition with activation of the ultrasound transducer for conveying acoustic energy.

In the embodiment described above with reference to the Figures, devices **10** and **80** comprise a cooling assembly including two independently-operable portions **22a** and **22b**,

22a being in thermal communication with sonotrode / RF applicator **18**. In some (non-depicted) embodiments, such devices comprise a cooling assembly including more than two independently-operable portions or only one portion. In some (non-depicted) embodiments, such devices are devoid of a cooling assembly.

5 In the embodiment described above with reference to the Figures, devices **10** and **80** comprise a cooling assembly including a cooling-fluid channel in thermal communication with sonotrode / RF applicator **18**. In some (non-depicted) embodiments, such devices comprise a cooling assembly including at least one cooling-channel that passes through the sonotrode / RF applicator **18**. In some (non-depicted) embodiments, such a device comprises
10 a cooling assembly devoid of cooling-channels.

 In the embodiment described above with reference to the Figures, devices **10** and **80** and the components thereof are together configured for the generation and directing longitudinal ultrasonic mechanical waves and of transverse ultrasonic mechanical waves. In some (non-depicted) embodiments, such devices are configured for generation and directing
15 only longitudinal ultrasonic mechanical waves. In some (non-depicted) embodiments, such devices are configured for generation and directing only transverse ultrasonic mechanical waves.

 The teachings herein have been described in the context of the treatment of subcutaneous fat in the hypodermis through the skin. In some embodiments, the teachings
20 herein are applied to the treatment of a volume of a material through a surface other than a skin surface and/or a material other than biological tissue.

 It is appreciated that certain features of the invention, which are, for clarity, described in the context of separate embodiments, may also be provided in combination in a single
25 embodiment. Conversely, various features of the invention, which are, for brevity, described in the context of a single embodiment, may also be provided separately or in any suitable subcombination or as suitable in any other described embodiment of the invention. Certain features described in the context of various embodiments are not to be considered essential features of those embodiments, unless the embodiment is inoperative without those elements.

30 Although the invention has been described in conjunction with specific embodiments thereof, it is evident that many alternatives, modifications and variations will be apparent to those skilled in the art. Accordingly, it is intended to embrace all such alternatives, modifications and variations that fall within the scope of the appended claims.

Citation or identification of any reference in this application shall not be construed as an admission that such reference is available as prior art to the invention.

Section headings are used herein to ease understanding of the specification and should not be construed as necessarily limiting.

CA-2,836,706

Submitted June 2016

CLAIMS

1. A device suitable for treatment of a volume of hypodermis with energy through a skin surface, the device comprising:

a sonotrode having an acoustic radiative surface and an ultrasound transducer functionally associated with the sonotrode and configured, when activated, to generate acoustic waves that are directed by said acoustic radiative surface into the volume of hypodermis for conveying an effective amount of acoustic energy into the volume of hypodermis for aesthetic modification thereof; and an RF energy source and an RF applicator having an RF radiative surface functionally associable with the RF energy source, said RF applicator being configured to direct RF waves generated by an activated RF energy source to said RF radiative surface to form a unipolar RF field for depositing an effective amount of thermal energy in the volume of hypodermis for aesthetic modification thereof, wherein the device is configured for activation of said ultrasound transducer and said RF energy source independently or concurrently; said sonotrode and said RF applicator are the same component whereby the acoustic radiative surface and the RF radiative surface are coupled to the same portion of the skin surface; and the radiative surface common to the sonotrode and the RF applicator comprises a layer of dielectric material, configured to serve as an insulator to prevent conduction of current through the RF radiative surface when coupled to an active RF energy source and as an acoustic matching layer when coupled to an active ultrasound transducer.

2. The device of claim 1, wherein said RF applicator is configured to direct RF waves having a frequency of not less than 2 MHz and said RF radiative surface is configured to form a unipolar RF field having a frequency of not less than 2 MHz.

3. The device of claim 1 or 2, wherein said sonotrode and said RF applicator are configured so that said volume of hypodermis treated at any one time is between 7 cm³ and

56 cm³.

4. The device of any one of claims 1 to 3, wherein said RF applicator is substantially a solid rigid mass of electrically-conductive material.

5

5. The device of any one of claims 1 to 4, wherein the device has multiple operating modes and wherein the acoustic energy source and the RF energy source are each activated either continuously or intermittently.

10

6. The device of claim 5, wherein the RF energy source is activated periodically at a rate of not less than 0.2 Hz.

15

7. The device of any one of claims 1 to 6, further comprising a cooling assembly configured, when activated, to cool at least one of said acoustic radiative surface and said RF radiative surface.

20

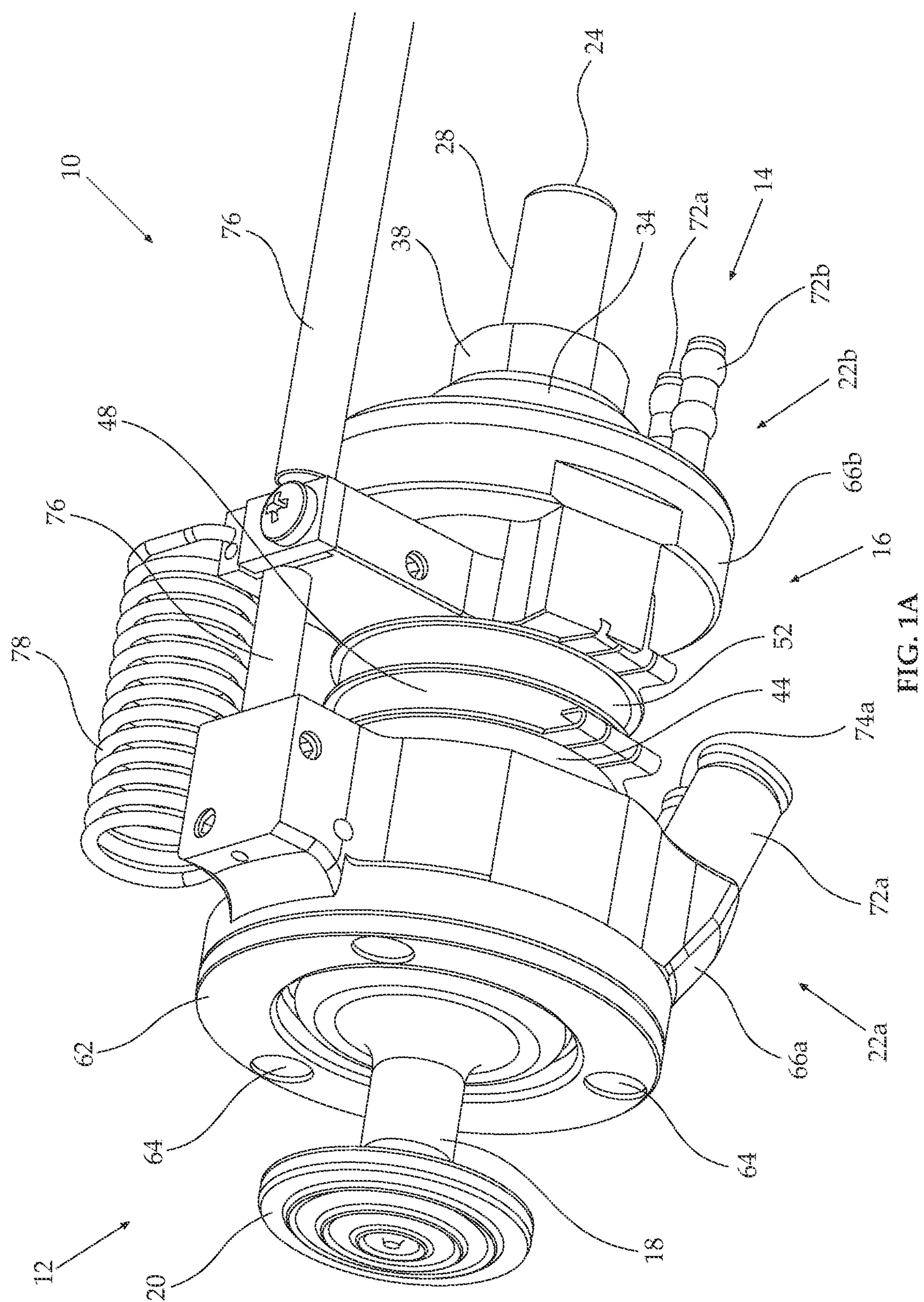
8. The device of any of claims 1 to 7, wherein said ultrasound transducer, said sonotrode and said acoustic radiative surface are together configured so that said acoustic energy is conveyed by at least one of longitudinal waves and transverse waves coupled into the hypodermis.

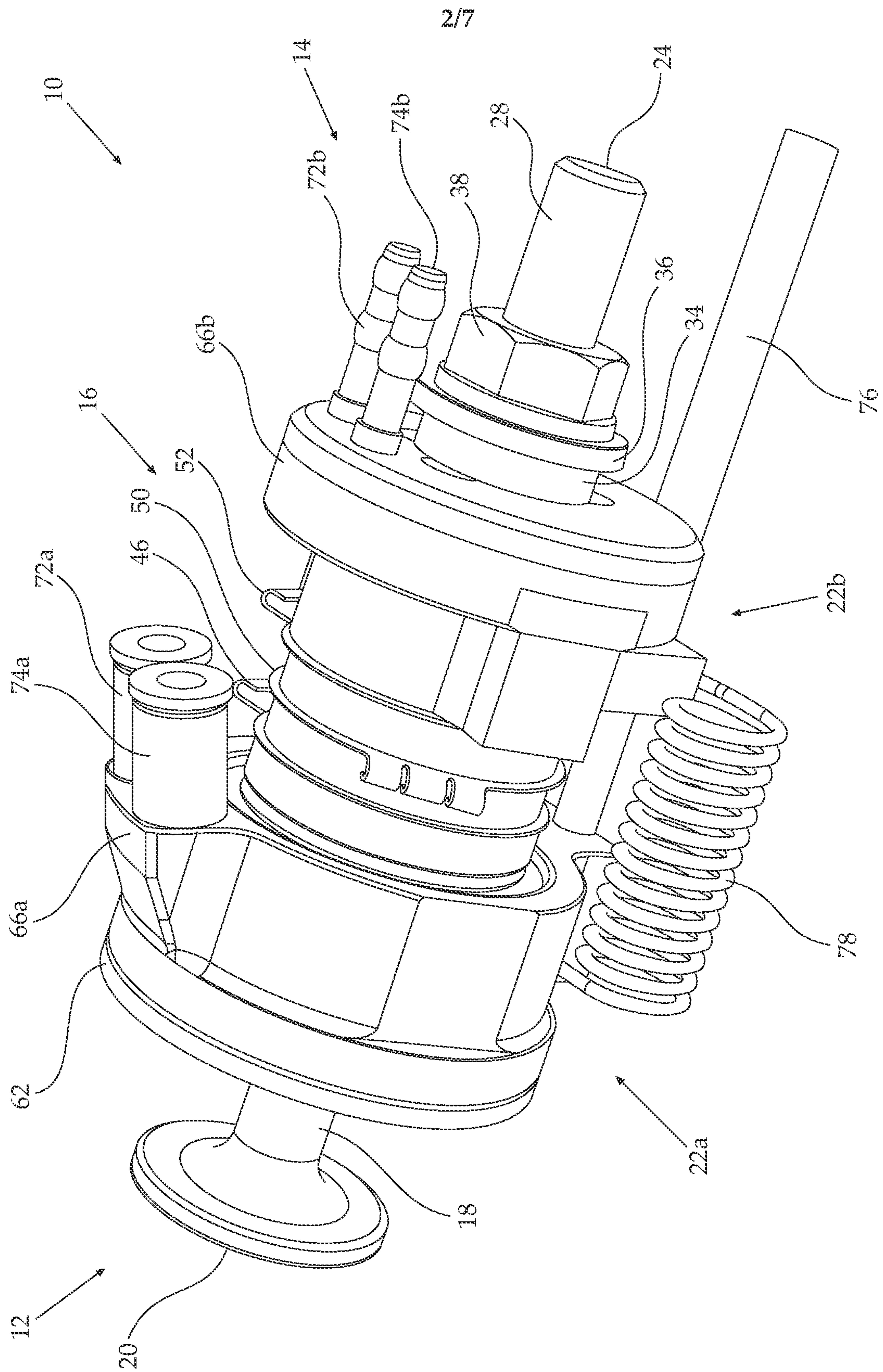
9. The device of claim 8, wherein both longitudinal and transverse waves are coupled into the hypodermis alternately.

25

10. A non-therapeutic method of using the device of any of claims 1 to 10 for cosmetic treatment of human skin, wherein the device is controlled to raise the temperature of the volume of hypodermis to above 42°C and to maintain it between 42°C and 48°C for a period of time.

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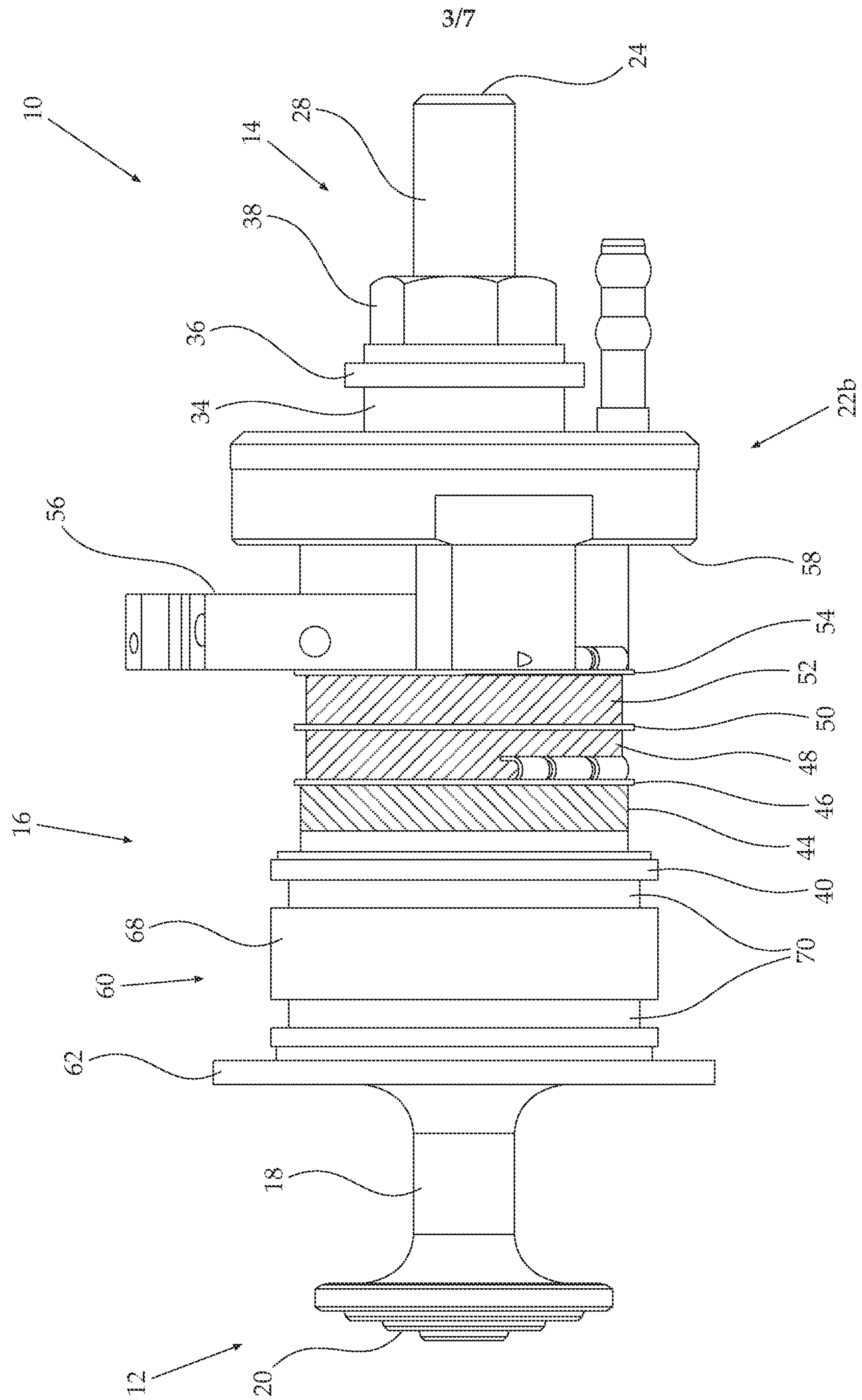


FIG. 1C

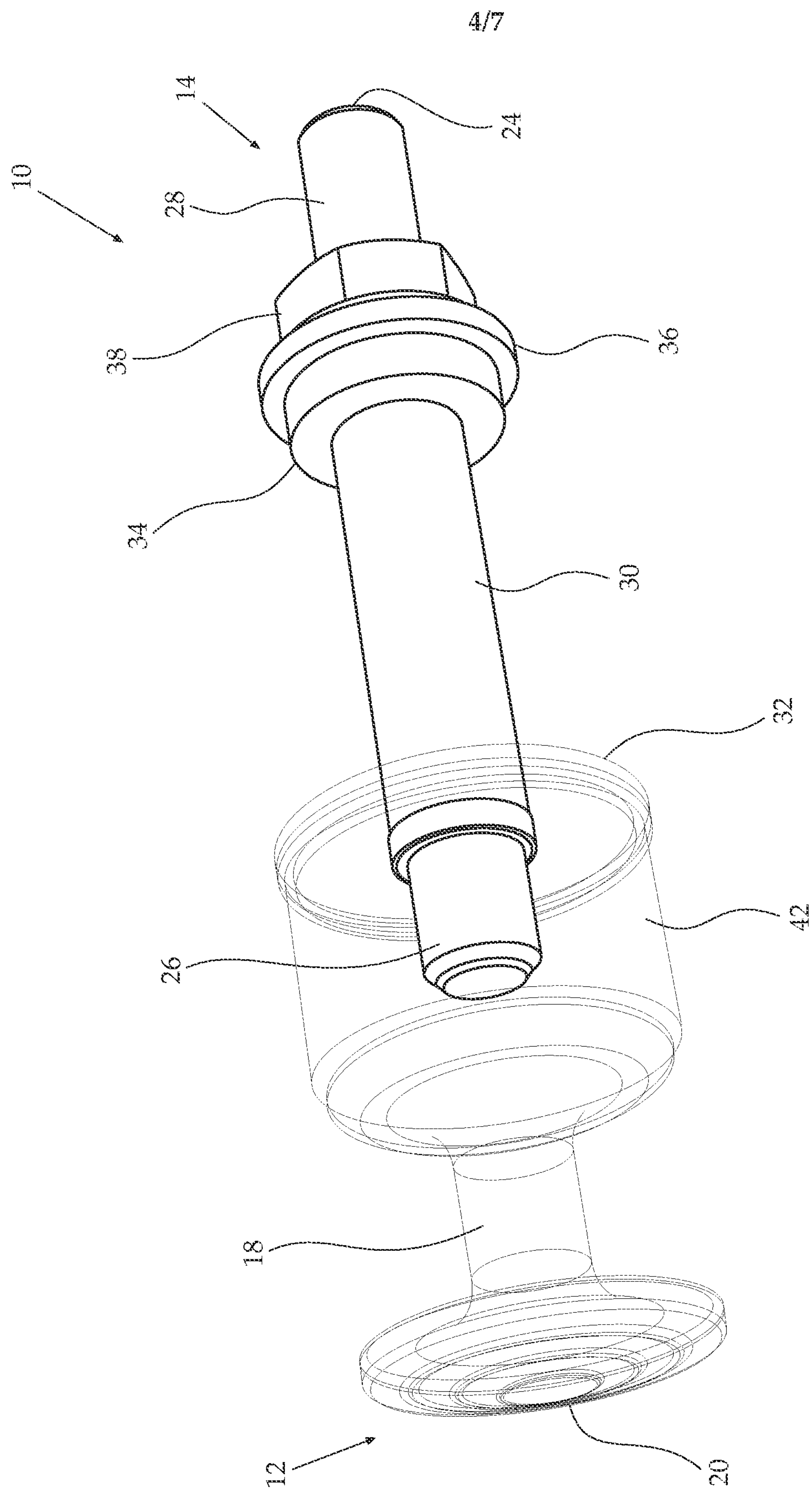


FIG. 1D

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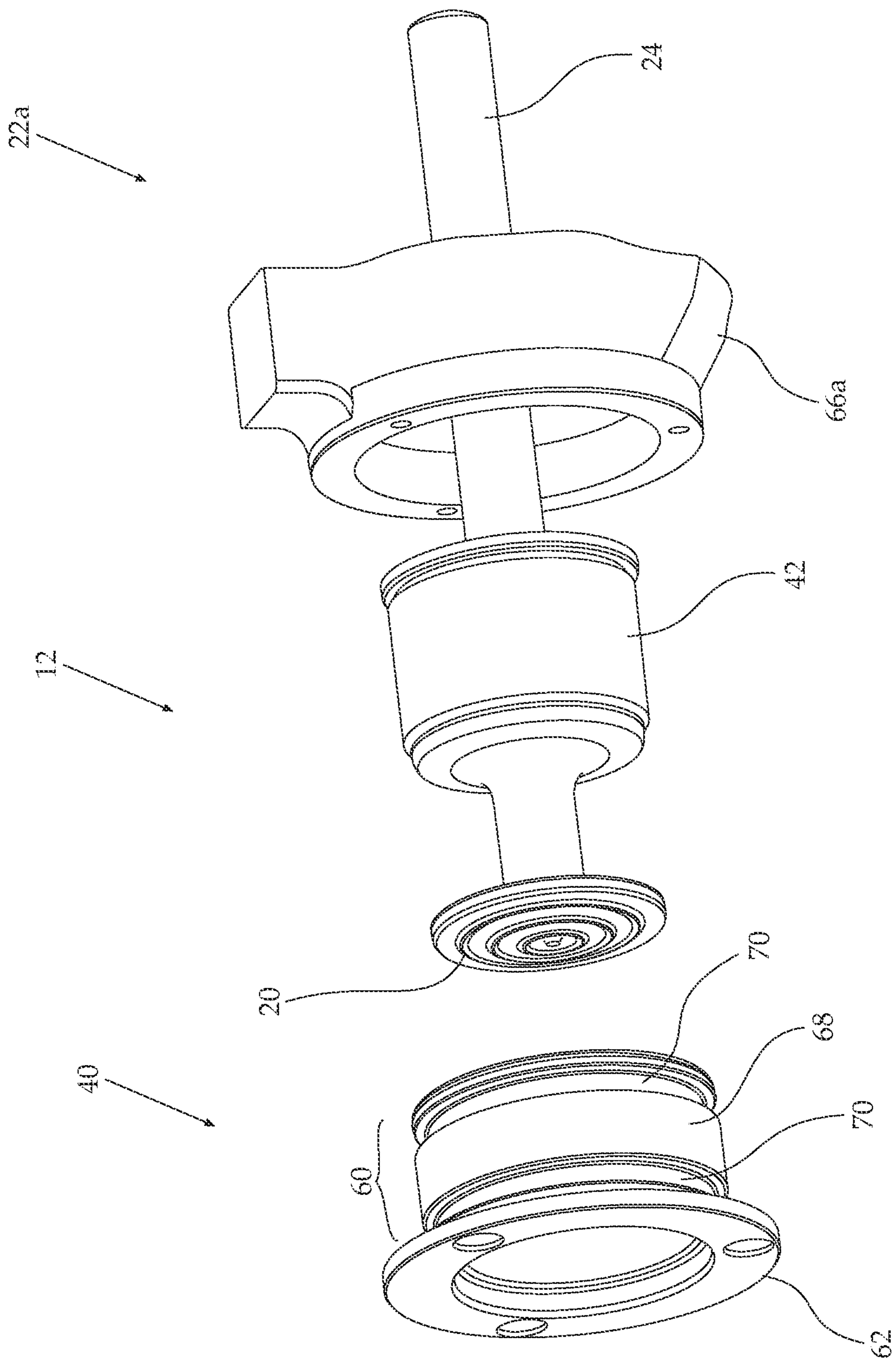


FIG. 1E

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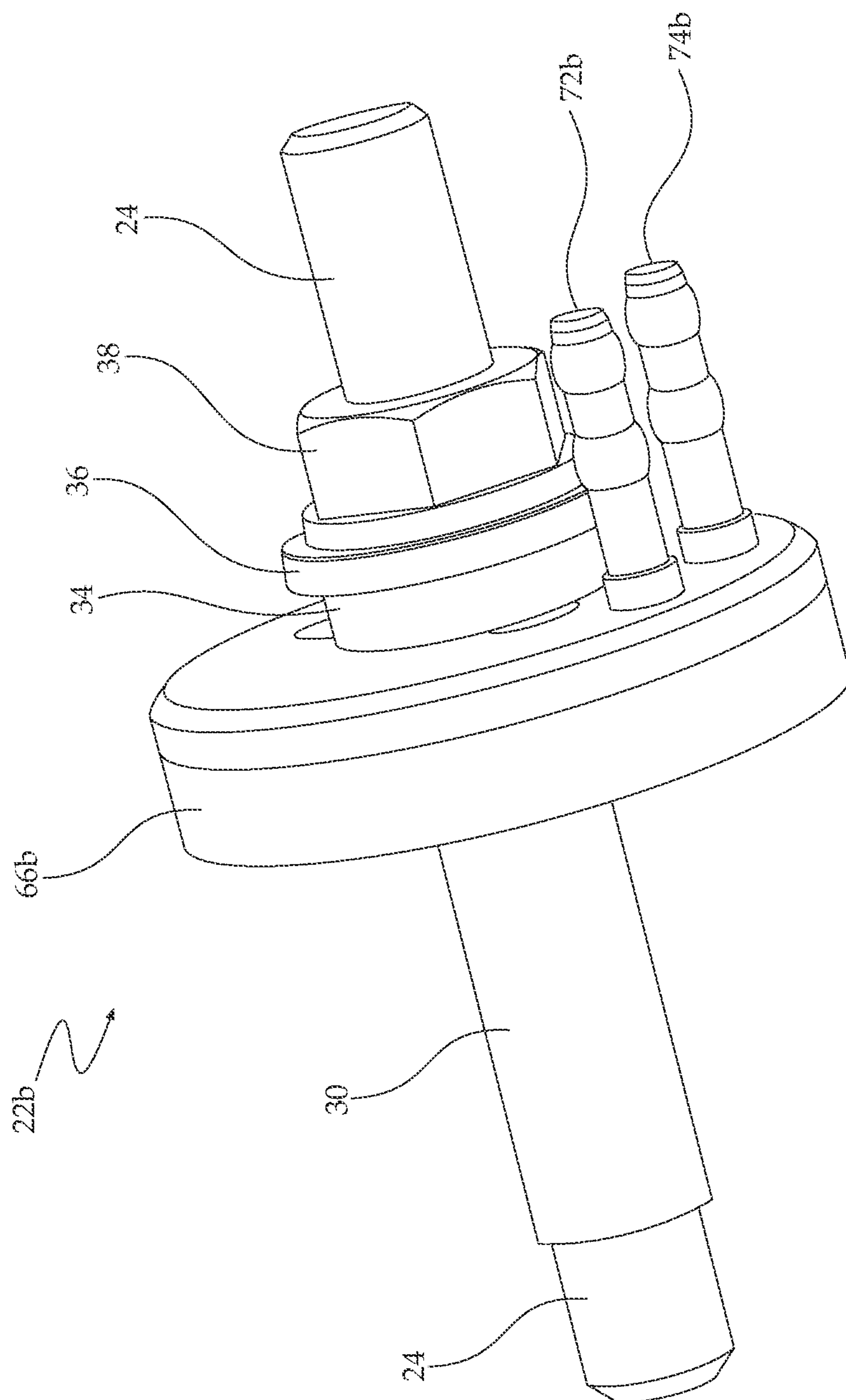


FIG. 1F

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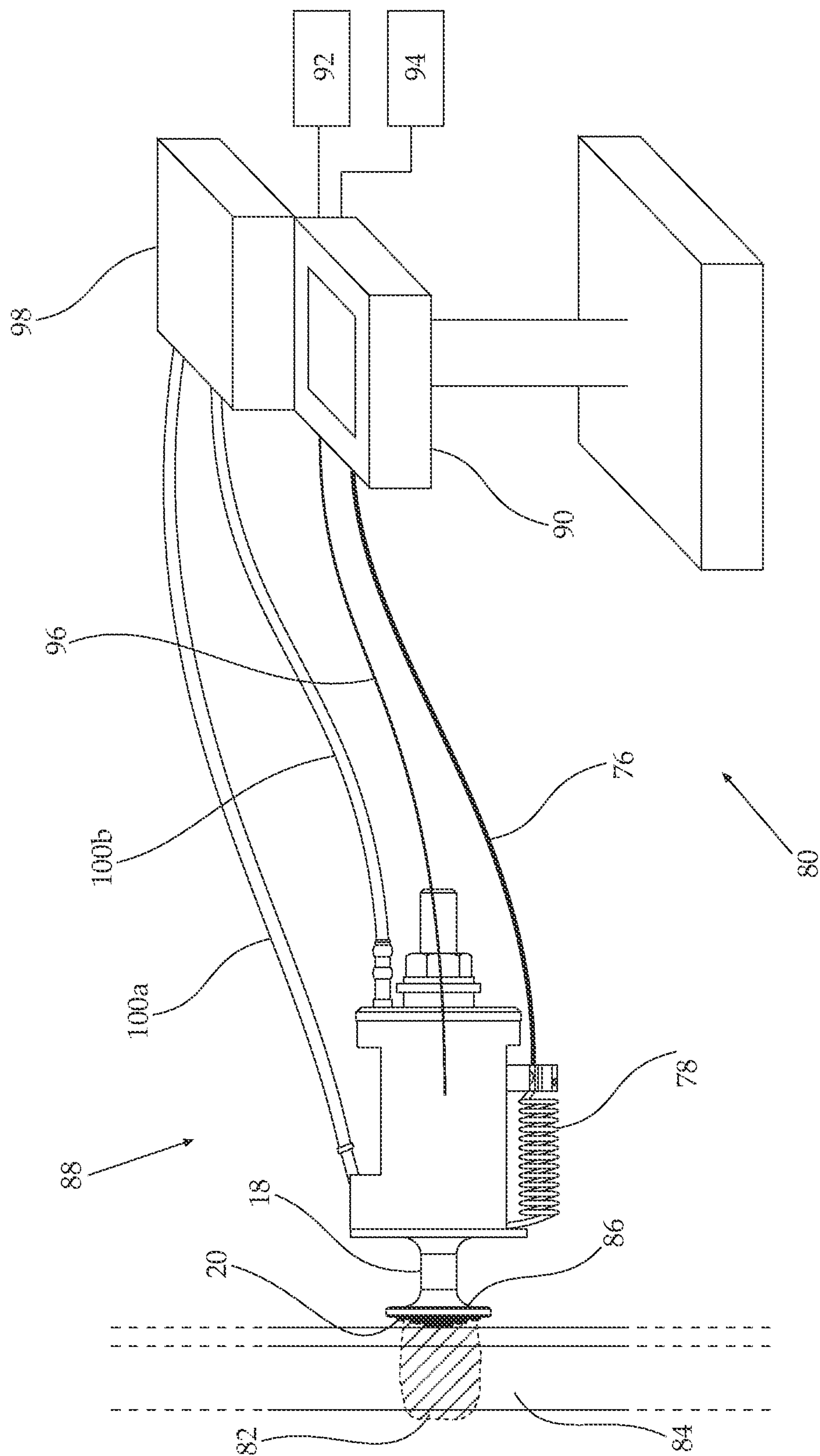


FIG. 2

