

(43) International Publication Date
28 November 2013 (28.11.2013)(51) International Patent Classification:
A61B 5/0428 (2006.01)(21) International Application Number:
PCT/IB2013/053947(22) International Filing Date:
15 May 2013 (15.05.2013)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:
61/651,173 24 May 2012 (24.05.2012) US(71) Applicant: **KONINKLIJKE PHILIPS N.V.** [NL/NL];
High Tech Campus 5, NL-5656 AE Eindhoven (NL).(72) Inventors: **REY, Eduardo Mario**; c/o High Tech Campus,
Building 5, NL-5656 AE Eindhoven (NL). **LIS, Bernard**;
c/o High Tech Campus, Building 5, NL-5656 AE Eindh-
hoven (NL).(74) Agents: **STEFFEN, Thomas** et al.; High Tech Campus,
Building 5, NL-5656 AE Eindhoven (NL).(81) Designated States (unless otherwise indicated, for every
kind of national protection available): AE, AG, AL, AM,
AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY,
BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DK, DM,
DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT,HN, HR, HU, ID, IL, IN, IS, JP, KE, KG, KM, KN, KP,
KR, KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD,
ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI,
NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU,
RW, SC, SD, SE, SG, SK, SL, SM, ST, SV, SY, TH, TJ,
TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, ZA,
ZM, ZW.(84) Designated States (unless otherwise indicated, for every
kind of regional protection available): ARIPO (BW, GH,
GM, KE, LR, LS, MW, MZ, NA, RW, SD, SL, SZ, TZ,
UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, RU, TJ,
TM), European (AL, AT, BE, BG, CH, CY, CZ, DE, DK,
EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV,
MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK, SM,
TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW,
ML, MR, NE, SN, TD, TG).**Declarations under Rule 4.17:**

- as to applicant's entitlement to apply for and be granted a patent (Rule 4.17(ii))
- as to the applicant's entitlement to claim the priority of the earlier application (Rule 4.17(iii))

Published:

- without international search report and to be republished upon receipt of that report (Rule 48.2(g))

(54) Title: REDUCTION OF MRI INTERFERENCE FROM THE ELECTROCARDIOGRAM USING LEAD INFORMATION

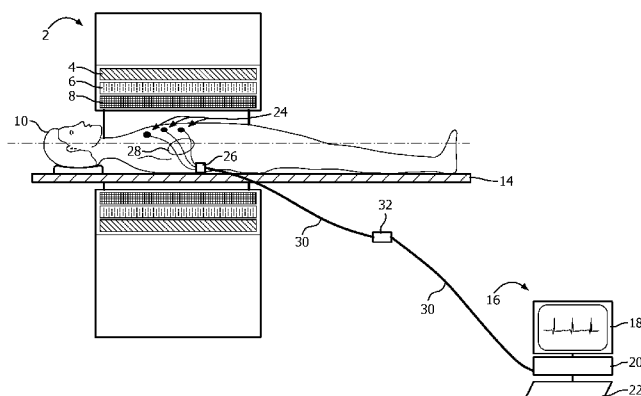


FIG. 1

(57) **Abstract:** A circuit (32) for use in an magnetic resonance (MR) system to reduce MR interference of a physiological signal $S(f)$ includes a first summing/subtraction node (36), a high pass filter (40), and a second summing/subtraction node (42). The first summing/subtraction node (36) inputs a first signal (34) including radio frequency magnetic interference $N(f)$ and a physiological signal $S(f)$, and a second signal (38) including the physiological signal $S(f)$ and an error signal $E(f)$, and subtractively combines the second signal with the first signal to generate a difference signal $N(f) - E(f)$. The high pass filter (40) filters the difference signal $N(f) - E(f)$ from the first summing/subtraction node. The second summing/subtraction node (42) subtractively combines the first signal $S(f) + N(f)$ (34) and the filtered signal $H(f) * [N(f) - E(f)]$ from the high pass filter, and generates the second signal $S(f) + E(f)$ (38).

REDUCTION OF MRI INTERFERENCE FROM THE ELECTROCARDIOGRAM USING LEAD INFORMATION

The following relates generally to medical imaging and patient monitoring. It finds particular application in conjunction with monitoring patients during magnetic resonance imaging and/or spectroscopy procedures, and will be described with particular reference thereto. However, it will be understood that it also finds application in other usage scenarios and is not necessarily limited to the aforementioned application.

In Magnetic Resonance (MR) Imaging, a subject is located in a static magnetic field. Magnetic resonance is excited in tissues of a subject by applying radio frequency (RF) pulses. Gradient magnetic fields or pulses are applied to the subject for spatial encoding, inducing gradient echoes, and the like. As the magnetic resonance in the subject decays, weak RF resonance signals are emitted. The weak RF resonance signals induce current in one or more coils which are used to reconstruct images.

During the imaging process, subjects often are monitored for physiological signs. The physiological monitoring provides monitoring of the vital signs for the subject. The physiological monitor can also be used to correct for motion or other artifacts.

In order to monitor the subject such as for pulse or heart rate, electrodes with lead wires are placed on the skin of the subject. The electrodes measure electrical activity to compute the heart rate or pulse. The lead wires from the electrodes are connected to a physiological device which converts the sensed electrical activity into a waveform signal such as the electrocardiogram signal (ECG). The waveform signal is transmitted along a wire, an optical medium, or wirelessly to a patient monitor or other like device.

Because the wires from the electrodes are electrically conductive, the lead wires and other wires are susceptible to interference currents induced by the gradient field pulses applied to the subject. The induced currents in the electrodes, the electrode lead wires, or a lead wire to the patient monitor, or a combination thereof produces gradient noise interference on the ECG signal. Interference from gradient pulses typically has an amplitude of about ± 100 mV but can reach as high as ± 10 V. An ECG typically has an amplitude of about 300 μ V to 5 mV peak-to-peak.

One approach to reducing MR interference is shielding. Heavy shielded cables can be used except for near the electrodes. Shielding the electrodes is difficult and expensive

and in most cases prohibitive due to leakage current limitations. Some approaches use fiber optic cable or wireless communication between the device which generates the physiological waveform and the patient monitor. However, interference still occurs at the electrode and the lead wires between the electrodes and the circuitry for converting the electrical ECG signal into light signal, or the like.

Another approach is to use filters. The analog ECG signal can be filtered in the analog domain. Alternatively, digital filtering can be performed after conversion of the analog signal to digital. However, additional firmware resources are needed and the digital signal processing dynamic ranges are often reduced which leads to performance issues and/or increased cost.

Another approach is to determine the theoretical gradient noise interference and use that information to subtract the expected interference from the ECG signal. For example, a connection to a gradient controller of a MR scanner can provide the identity and timing of each gradient field applied to the subject. However, the predicted interference based on the generated sources of interference (e.g. measure of generated gradient fields) and the actual interference on each wire lead or lead cable can vary with electrode placement and the like.

The following discloses a new and improved reduction of MRI interference from the ECG using lead (or electrode) information which addresses the above referenced issues, and others.

In accordance with one aspect, a circuit for use in an magnetic resonance (MR) system to reduce MR interference of a physiological signal $S(f)$ includes a first summing/subtraction node, a high pass filter, and a second summing/subtraction node **(42)**. The first summing/subtraction node inputs a first signal including all interference components generated by the MRI scanner $N(f)$ and a physiological signal $S(f)$, and a second signal including the physiological signal $S(f)$ and an error signal $E(f)$, and subtractively combines the second signal with the first signal to generate a difference signal $N(f) - E(f)$. The high pass filter filters the difference signal $N(f) - E(f)$ from the first summing/subtraction node. The second summing/subtraction node subtractively combines the first signal $S(f) + N(f)$ and the filtered signal $H(f) * [N(f) - E(f)]$ from the high pass filter, and generates the second signal $S(f) + E(f)$.

In accordance with another aspect, a method for use in an MR system to reduce MR interference of a physiological signal $S(f)$ includes inputting **(46)** a first signal **(34)** which includes all interference components generated by the MRI scanner $N(f)$ and a

physiological signal $S(f)$. The second signal **(38)** $S(f)+E(f)$ including the physiological signal $S(f)$ and an error signal $E(f)$ is combined subtractively from the first signal $S(f)+N(f)$, and generates a difference signal $N(f)-E(f)$. The difference signal is filtered using a high pass filter. The first signal $S(f)+N(f)$ and the filtered signal $H(f) * [N(f)-E(f)]$ from the high pass filter are combined subtractively, and generate the second signal $S(f)+E(f)$.

In accordance with another aspect, a circuit for use in an magnetic resonance (MR) system to reduce MR interference of a physiological signal $S(f)$ includes a lead, a feed forward path, and a node. The lead carries an input signal including $S(f)$ contaminated with $N(f)$. The feed forward path feeds forward $N(f)$ in a feed forward circuit. The node subtractively combines the input signal and the feed forward signal to generate an output signal.

One advantage is reduced MR gradient interference.

Another advantage resides in removal of interference in hardware before analog-to-digital conversion.

Another advantage resides in using actual interference itself to correct the ECG signal for gradient interference.

Another advantage resides in maintaining the physiological waveform morphology.

Another advantage is a more robust physiological signal quality independent of the scan sequence.

Another advantage is more reliable cardiac gating performance.

Another advantage is not requiring additional electrodes, lead wires, gauss sensors, or the like to capture the interference components generated by the MRI scanner.

Still further advantages will be appreciated to those of ordinary skill in the art upon reading and understanding the following detailed description.

The invention may take form in various components and arrangements of components, and in various steps and arrangement of steps. The drawings are only for purposes of illustrating the preferred embodiments and are not to be construed as limiting the invention.

FIGURE 1 diagrammatically illustrates an embodiment of the interference reduction circuit disposed in a Magnetic Resonance Imaging system.

FIGURE 2 diagrammatically illustrates another embodiment of the circuit disposed in a Magnetic Resonance Imaging system

FIGURE 3 diagrammatically illustrates an embodiment of the interference reduction circuit in a block diagram.

FIGURE 4 schematically illustrates an embodiment of the circuit in a circuit diagram.

5 FIGURE 5 graphically illustrates an ECG waveform with reduced MR interference.

FIGURE 6 flowcharts one method of using an embodiment of reducing MR interference on a lead.

10 With reference to FIGURE 1, an embodiment of the interference reduction circuit disposed in a Magnetic Resonance Imaging system is diagrammatically illustrated. The system includes a MR scanner **2** in a cross section view. The scanner **2** includes a main magnet **4**, one or more gradient coils **6**, and one or more radio frequency (RF) coils **8**. The main magnet **4** generates a static or B_0 magnetic field. The RF coils generate RF pulses which excite and manipulate magnetic resonance in a subject **10**. The one or more gradient coils **6** generate gradient magnetic fields across the static magnetic field spatially encode the induced resonance, induced gradient echoes, and the like. The scanner includes an opening **12** or bore that defines an examination region in which the subject **10** is placed for a spectroscopic and/or imaging examination. The subject is supported by a subject support such as padding **14**.

20 The subject is monitored by a monitoring device **16**. The monitoring device **16** includes a display **18**, one or more processors **20**, and can include at least one input device **22**. The display **18** displays the monitored waveforms such as ECG. The one or more processors provide analog to digital signal conversion, filtering, formatting for display of the signal. The monitoring device can include keypad, keyboard, mouse, etc., for entry of information about the subject, and commands to drive the monitoring device. The monitoring device can be connected to a hospital information system (HIS) and the like.

30 One or more sensors, such as ECG electrodes **24** are attached to the subject to monitor physiological signals from the body surface. The ECG electrodes **24** can be attached with a temporary adhesive that adheres to the skin to sense heart related electrical activity. The electrodes **24** connect to a physiological device **26** by small wires **28** which generates a waveform signal such as an ECG signal. The generated waveform signal is transmitted between the physiological device **26** and the monitoring device **16** via a cable **30**. A interference reduction circuit **32** is disposed along the cable **30**. The circuit **32** can be disposed at either end or in the middle of the cable. The circuit **32** inputs a signal which

includes the waveform signal and interference from the magnetic resonance gradient pulses. The circuit 32 outputs the physiological signal with reduced or removed magnetic interference. The circuit can connect to the physiological device, patient monitor, and/or the cable using standard hardware interfaces such that the circuit can be used with existing devices.

In an alternate embodiment, the circuit 32 can be included in either the physiological device 26 or the monitoring device 20. Incorporating the circuit into one of the devices is advantageous where the signal is transmitted wirelessly or fiber optically. Alternatively the circuit can be included in the cable, a connector, a separate adapter, and/or any combination.

A 'processor' as used herein encompasses an electronic component which is able to execute a program or machine executable instruction. References to the computing device comprising "a processor" should be interpreted as possibly containing more than one processor or processing core. The processor may for instance be a multi-core processor. A processor may also refer to a collection of processors within a single computer system or distributed amongst multiple computer systems. The term computing device should also be interpreted to possibly refer to a collection or network of computing devices each comprising a processor or processors. Many programs have their instructions performed by multiple processors that may be within the same computing device or which may even be distributed across multiple computing devices.

A 'hardware interface' as used herein encompasses an interface which enables the processor of a computer system to interact with and/or control an external computing device and/or apparatus. A hardware interface may allow a processor to send control signals or instructions to an external computing device and/or apparatus. A hardware interface may also enable a processor to exchange data with an external computing device and/or apparatus. Examples of a hardware interface include, but are not limited to: a universal serial bus, IEEE 1394 port, parallel port, IEEE 1284 port, serial port, RS-232 port, IEEE-488 port, Bluetooth connection, Wireless local area network connection, TCP/IP connection, Ethernet connection, control voltage interface, MIDI interface, analog input interface, and digital input interface.

A 'display' or 'display device' as used herein encompasses an output device or a user interface adapted for displaying images or data. A display may output visual, audio, and or tactile data. Examples of a display include, but are not limited to: a computer monitor, a television screen, a touch screen, tactile electronic display, Braille screen, Cathode ray tube

(CRT), Storage tube, Bistable display, Electronic paper, Vector display, Flat panel display, Vacuum fluorescent display (VF), Light-emitting diode (LED) displays, Electroluminescent display (ELD), Plasma display panels (PDP), Liquid crystal display (LCD), Organic light-emitting diode displays (OLED), a projector, and Head-mounted display.

5 Magnetic Resonance (MR) data is defined herein as being the recorded measurements of radio frequency signals emitted by atomic spins by the antenna of a Magnetic resonance apparatus during a magnetic resonance imaging scan. A Magnetic Resonance Imaging (MRI) image is defined herein as being the reconstructed two or three dimensional visualization of anatomic data contained within the magnetic resonance imaging
10 data. This visualization can be performed using a computer.

FIGURE 2 diagrammatically illustrates another embodiment of the interference reduction circuit **32** disposed in a Magnetic Resonance Imaging system. The circuit **32** is electrically connected with each of the wire leads **28** from the electrodes **24** affixed to the subject **10** to the physiological device **26**. Each wire lead **28** is filtered using the
15 circuit **32** to generate the reduced interference physiological waveform. The physiological device **26** communicates with the patient monitor **16** wirelessly.

FIGURE 3 diagrammatically illustrates an embodiment of the interference reduction circuit **32** in a block diagram. The circuit inputs a signal **34** which includes a physiological signal and interference from magnetic resonance such as gradient pulses. The
20 physiological signal is represented by $S(f)$, and the interference or noise of the magnetic resonance represented by $N(f)$. The circuit includes a first summing/subtraction node **36** which receives the input signal **34**, $S(f) + N(f)$ and a second or feedback signal **38** which includes the physiological signal and an error component, $S(f) + E(f)$. The first node **36** subtracts the second signal **38** from the input signal **34** which is then fed to a high pass filter
25 **40** such as a Sallen-Key filter. The high pass filter **40** seeks to preserve the interference signal $N(f)$ and minimize an error component $E(f)$. The filtered signal from the high pass filter **40**, $H(f) * [N(f) - E(f)]$, is input or fed forward into a second summing/subtraction node **42**. The second node **42** subtracts the signal from the high pass filter, $H(f) * [N(f) - E(f)]$ from the original input signal **34**, $S(f) + N(f)$, which generates the second signal **38**, $S(f) + E(f)$. The
30 second signal **38** includes the physiological signal and the error component which are fed back into the first node **36**. The error feedback process minimizes the error signal, $E(f)$, such that the output signal **39** of the circuit is the physiological signal.

The interference reduction circuit can convert the output signal to a digital waveform for further processing, filtering, or display as the physiological signal on the

display **18**. Prior to the analog-to-digital conversion other options can be included such as low pass filtering, slew-rate limiting, or interpolation stages or any combination thereof. The low pass filter can reduce or eliminate the high frequency component remaining from the subtraction process at the second node **42**. The interference reduction circuit can further
5 include an electro-optical transducer, an RF transmitter or the like to convert the output signal **39** to a non-electrical format.

FIGURE 4 schematically illustrates an embodiment of the interference reduction circuit **32** in a circuit diagram. The illustrated embodiment includes an ECG filter with an ECG lead input. The ECG lead **28** includes the physiological signal, **34** e.g. ECG
10 signal, and the magnetic resonance interference such as from gradient pulses. The first node **36** includes an operational amplifier and discrete components, and inputs the signal **34** from the lead and subtracts a second signal **38** which includes the ECG signal and an error component. The remaining signal which includes the noise or interference component and the error component is fed into the high pass filter **40**. The high pass filter **40** includes an
15 operational amplifier and discrete components. The output signal of the high pass filter is fed into the second node **42**. The second node **42** subtracts the output of the high pass filter from the input signal **34** which leaves the physiological signal and the error component and then feeds back the second signal **38** to the first node **36** to minimize the error component $E(f)$. The second node **42** includes an operational amplifier and discrete components. The second
20 signal **38** is fed into an optional low pass filter **44**. The output from the low pass filter forms the output **39** from the circuit. The low pass filter includes an operational amplifier and discrete components. The circuit of this embodiment can be implemented with a quad amp package with discrete components.

FIGURE 5 graphically illustrates an ECG waveform with reduced MR
25 interference. The overall peak to peak ECG signal is not decreased and the noise of the gradient pulse is reduced. The gradient pulses result in about 2 mV of the noise on the ECG signal. The cause of the remaining noise is the start and finish of the gradient sequences, which are likely due to the head and tail of the high pass filter.

FIGURE 6 flowcharts one method of using an embodiment of reducing MR
30 interference on a lead. In a step **46**, the signal **34** from a lead wire or electrode wire is input. The signal **34** includes the physiological signal $S(f)$ such as ECG and interference $N(f)$ from magnetic resonance imaging such as from gradient pulses. In an iterative series of steps, beginning with a step **48**, the second signal **38** which includes the physiological signal $S(f)$ and the error component $E(f)$ is subtracted from the input signal **34** at the node **36**. The

subtracted signal $S(f) + N(f) - [S(f) + E(f)]$ is filtered to isolate the interference using the high pass filter **40** in a step **50**. The high pass filter preserves the noise or interference $N(f)$ from the magnetic resonance imaging. The filtered signal $H(f) \cdot [N(f) - E(f)]$ is subtracted from the input signal **34** at node **42** in a step **52**, and the physiological signal $S(f)$ and the error component $E(f)$ are fed back into the earlier step **48** of subtracting by the node **36** the second signal from the input signal. The feedback and subtracting processes minimize the error component leaving only the physiological signal $S(f)$ such as the ECG signal.

In an optional step **54**, the second signal **38** is filtered using the low pass filter **44**. The output of the filter can then be converted from an analog waveform to digital waveform in a step **56**. The analog-to-digital conversion can be optionally included in the circuit **32** or separate. The signal can be transmitted wirelessly, optically, or via wired connection or the like to the patient monitor.

It is to be appreciated that in connection with the particular illustrative embodiments presented herein certain structural and/or function features are described as being incorporated in defined elements and/or components. However, it is contemplated that these features may, to the same or similar benefit, also likewise be incorporated in other elements and/or components where appropriate. It is also to be appreciated that different aspects of the exemplary embodiments may be selectively employed as appropriate to achieve other alternate embodiments suited for desired applications, the other alternate embodiments thereby realizing the respective advantages of the aspects incorporated therein.

It is also to be appreciated that particular elements or components described herein may have their functionality suitably implemented via hardware, software, firmware or a combination thereof. Additionally, it is to be appreciated that certain elements described herein as incorporated together may under suitable circumstances be stand-alone elements or otherwise divided. Similarly, a plurality of particular functions described as being carried out by one particular element may be carried out by a plurality of distinct elements acting independently to carry out individual functions, or certain individual functions may be split-up and carried out by a plurality of distinct elements acting in concert. Alternately, some elements or components otherwise described and/or shown herein as distinct from one another may be physically or functionally combined where appropriate.

In short, the present specification has been set forth with reference to preferred embodiments. Obviously, modifications and alterations will occur to others upon reading and understanding the present specification. It is intended that the invention be construed as including all such modifications and alterations insofar as they come within the scope of the

appended claims or the equivalents thereof. That is to say, it will be appreciated that various of the above-disclosed and other features and functions, or alternatives thereof, may be desirably combined into many other different systems or applications, and also that various presently unforeseen or unanticipated alternatives, modifications, variations or improvements
5 therein may be subsequently made by those skilled in the art which are similarly intended to be encompassed by the following claims.

CLAIMS:

What is claimed is:

1. A circuit **(32)** for use in an magnetic resonance (MR) system to reduce MR interference of a physiological signal $S(f)$, the circuit comprising:

a first summing/subtraction node **(36)** which inputs a first signal **(34)** including all interference components generated by the MRI scanner $N(f)$ and a physiological signal $S(f)$, and a second signal **(38)** including the physiological signal $S(f)$ and an error signal $E(f)$, and which subtractively combines the second signal $S(f)+E(f)$ with the first signal $S(f)+N(f)$ to generate a difference signal $N(f)-E(f)$;

a high pass filter **(40)** which filters the difference signal $N(f)-E(f)$ from the first summing/subtraction node; and

a second summing/subtraction node **(42)** which subtractively combines the first signal $S(f)+N(f)$ **(34)** and the filtered signal $H(f) * [N(f)-E(f)]$ from the high pass filter, and generates the second signal $S(f)+E(f)$ **(38)**.

2. The circuit **(32)** according to claim 1, further including at least one of:

a low pass filter **(44)**;

a slew-rate limit unit; and

an interpolation unit.

3. The circuit **(32)** according to either one of claims 1 and 2, wherein the first summing/subtraction node **(36)**, the second summing/subtraction node **(42)**, and the high pass filter **(40)** each include an operational amplifier.

4. The circuit **(32)** according to any one of claims 1-3, wherein the physiological signal includes an electrocardiogram (ECG) signal.

5. The circuit **(32)** according to any one of claims 1-4, further including:

an analog to digital converter which converts the second signal to a digital signal.

6. The circuit **(32)** according to any one of claims 1-5, wherein the high pass filter **(40)** includes a Sallen-Key filter.
7. The circuit **(32)** according to any one of claims 1-6, wherein the radio frequency magnetic resonance interference includes gradient pulse interference.
8. An electrocardiographic system comprising:
 - at least one electrode **(24)**;
 - at least one wire **(28)**, each wire connected to an electrode **(24)**;
 - the circuit **(32)** of any one of claims 1-7 connected to the at least one wire to remove the magnetic resonance interference $N(f)$.
9. The system according to claim 8, wherein each at least one wire is connected to a separate circuit **(32)**.
10. The system according to either one of claims 8 and 9, further including:
 - at least one patient monitor **(16)** which receives the physiological signal $S(f)$ with reduced magnetic resonance interference
11. A method for use in an MR system to reduce MR interference of a physiological signal $S(f)$, the method comprising:
 - inputting **(46)** a first signal **(34)** which includes all interference components generated by the MRI scanner $N(f)$ and a physiological signal $S(f)$;
 - combining subtractively **(48)** a second signal **(38)** $S(f)+E(f)$ including the physiological signal $S(f)$ and an error signal $E(f)$ from the first signal $S(f)+N(f)$, and generating a difference signal $N(f)-E(f)$,
 - filtering **(50)** the difference signal using a high pass filter **(40)**;
 - combining subtractively **(52)** first signal $S(f)+N(f)$ **(34)** and the filtered signal $H(f) * [N(f)-E(f)]$ from the high pass filter, and generates the second signal $S(f)+E(f)$ **(38)**.
12. The method according to claim 11, further including:
 - filtering **(54)** the second signal **(38)** using a low pass filter **(44)**.

13. The method either one of claims 11 and 12, wherein the first signal **(36)** include a physiological signal.
14. The method according to any one of claims 11-13, further including:
converting the second signal from an analog waveform to a digital waveform.
15. The method according to any one of claims 11-14, wherein the method is performed on each of a plurality of electrocardiogram (ECG) electrode leads **(28)**.
16. The method according to any one of claims 11-15, wherein filtering includes slew rate limiting.
17. A non-transitory computer-readable storage medium carrying software which controls one or more electronic data processing devices to perform the method according to any one of claims 11-16.
18. An electronic data processing device configured to perform the method according to any one of claims 11-16.
19. A circuit for use in an magnetic resonance (MR) system to reduce MR interference of a physiological signal $S(f)$, the circuit comprising:
a lead **(30)** which carries an input signal including $S(f)$ contaminated with an interference signal $N(f)$;
a feed forward path **(36,40)** which feeds forward the interference signal $N(f)$ in a feed forward circuit;
a node **(40)** which subtractively combines the input signal $S(f)+N(f)$ and the feed forward interference signal $N(f)$ to generate an output signal $S(f)$.
20. The circuit according to claim 19, wherein the output signal includes $S(f)$ and an error component $E(f)$ and further including:
a feedback circuit which feeds back the output signal $S(f)+E(f)$ to the feed forward path to minimize the error component $E(f)$; and

a second node **(36)** which subtractively combines the fed back output signal $S(f) + E(f)$ and the input signal $S(f) + N(f)$ such that the feed forward signal includes the interference signal and the error signal $N(f)$ and $E(f)$.

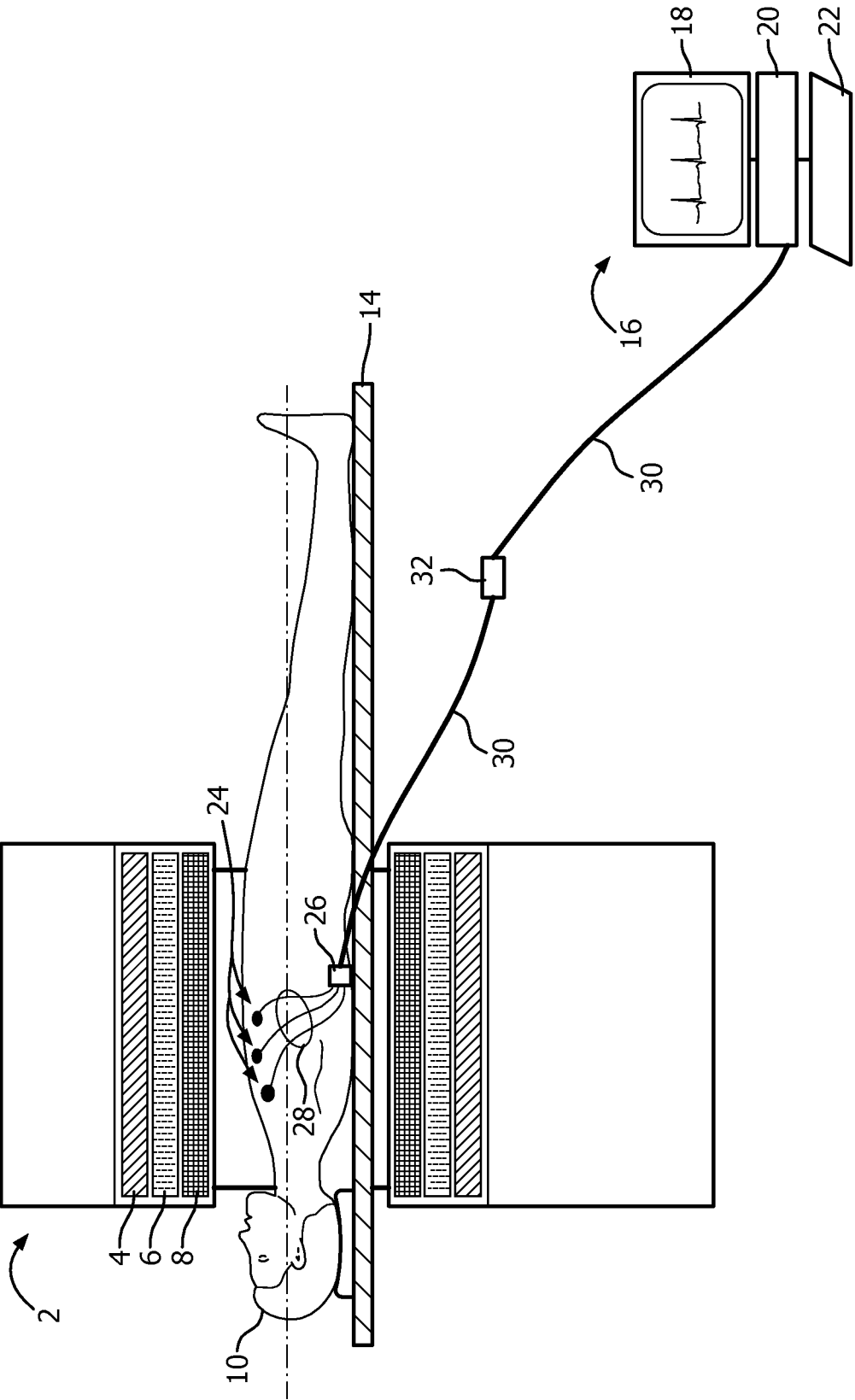


FIG. 1

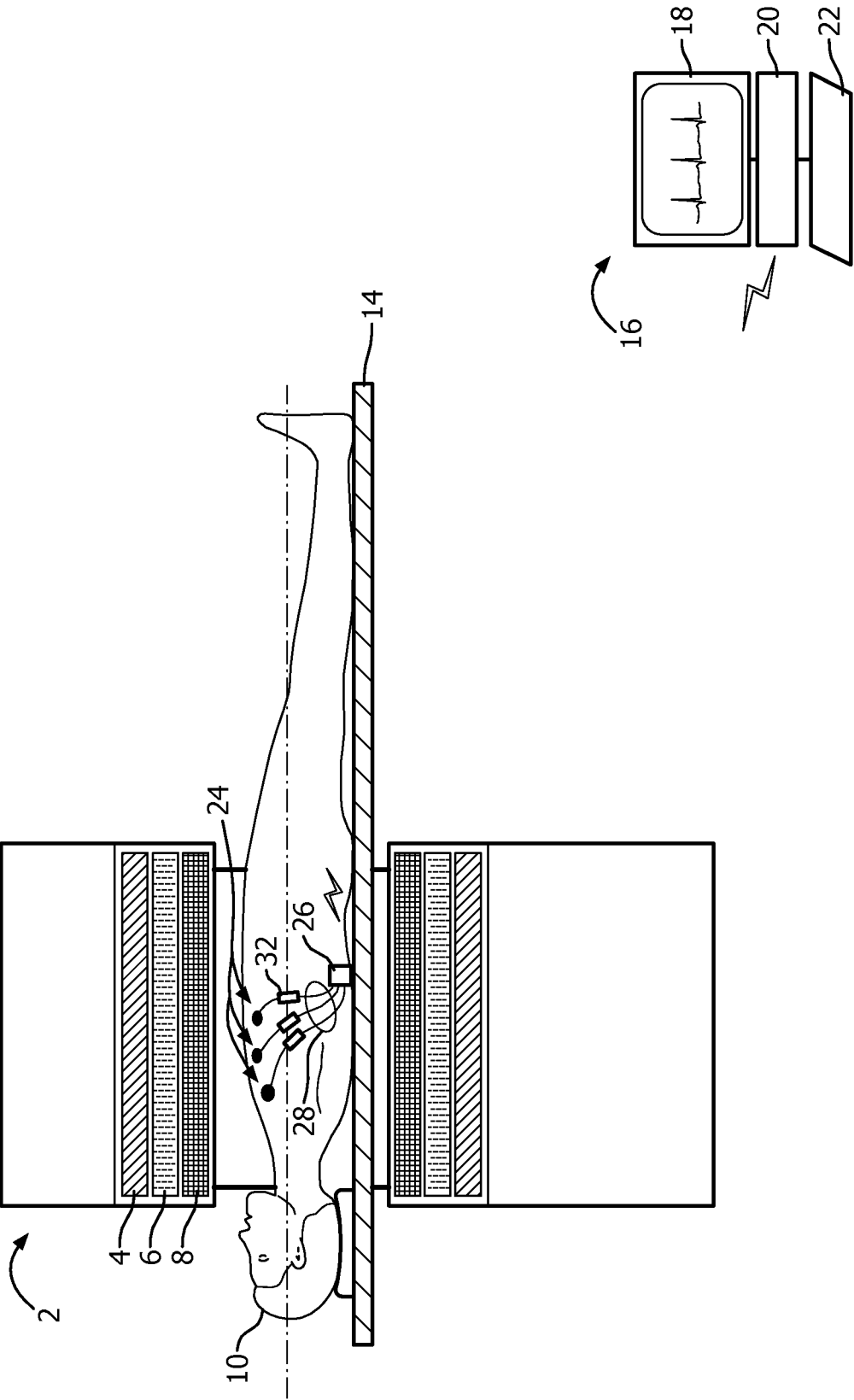


FIG. 2

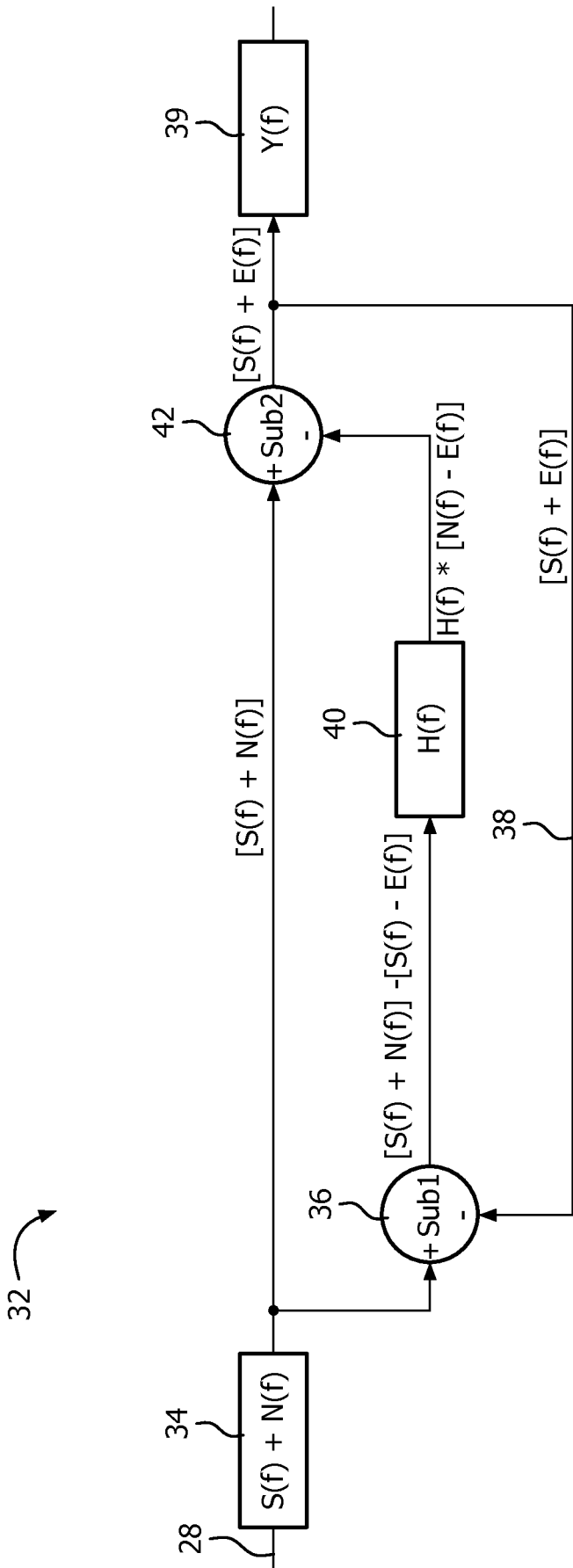


FIG. 3

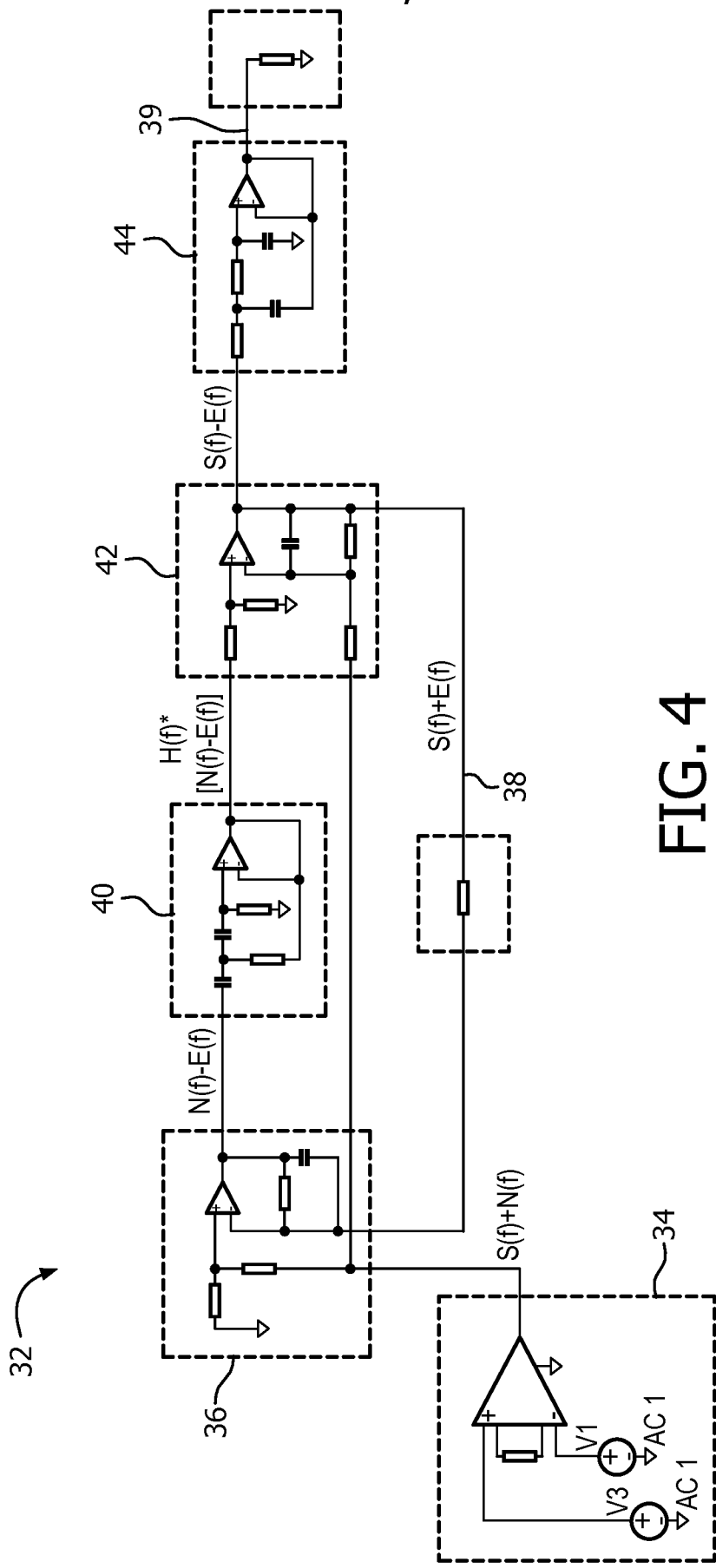


FIG. 4

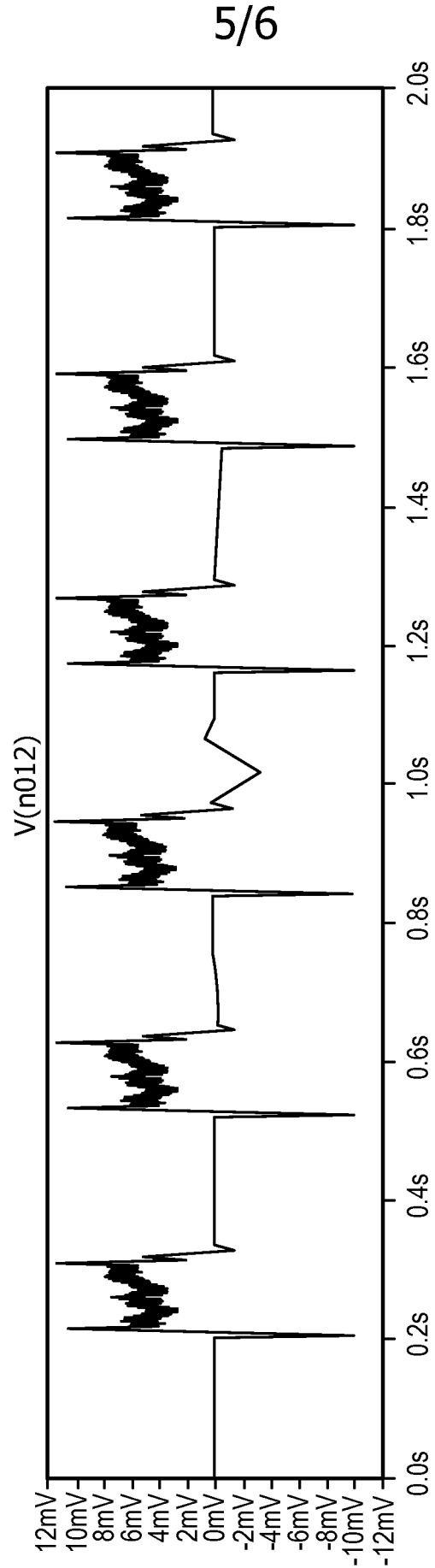


FIG. 5

6/6

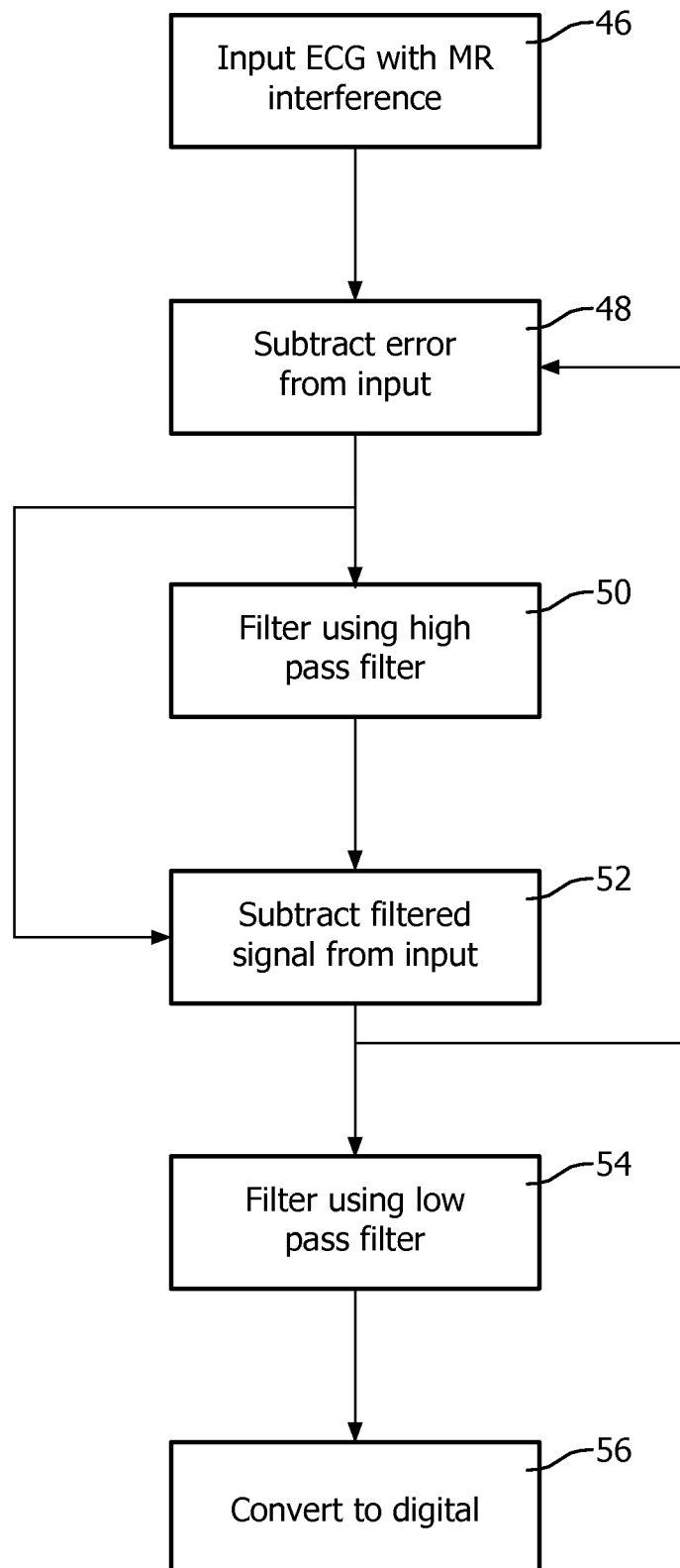


FIG. 6