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CREST FACTOR ENHANCEMENT IN
ELECTROSURGICAL GENERATORS

ABSTRACT

The present disclosure relates to an electrosurgical generator (20) which includes a controller (24) configured to generate a first pulse train (60) having at least one first control pulse (60a) and at least one first reset pulse (60b). The controller
5 (24) also includes a second pulse train (62) having at least one second control pulse (62a) and at least one second reset pulse (62b). The first control pulse(s) and the second control pulse(s) are asynchronous and the reset pulse(s) are synchronous. The electrosurgical generator (20) also includes an RF output stage (28) which includes a first switching element and a second switching element. The control pulses are
10 configured to activate the first switching element and second switching elements, respectively, in an asynchronous fashion to generate a non-continuous RF waveform.

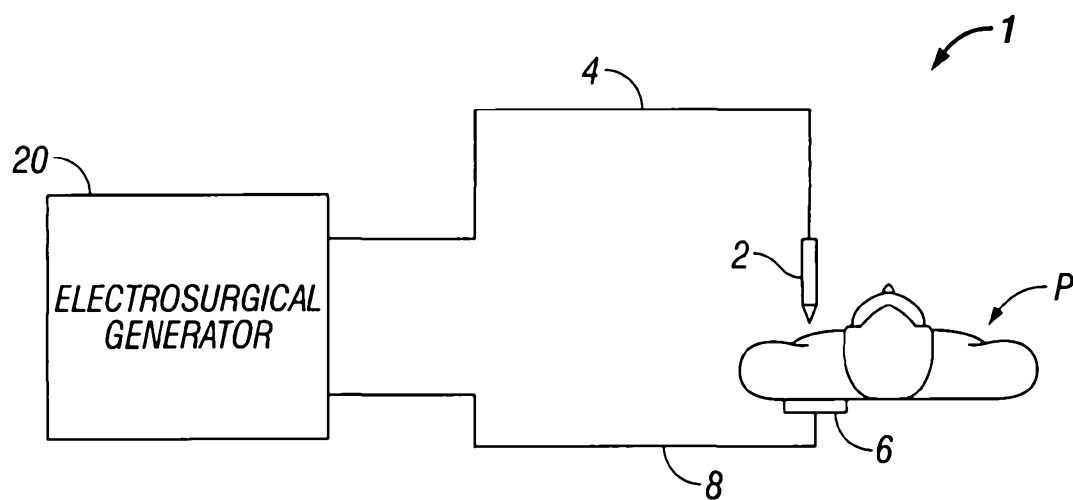


FIG. 1A

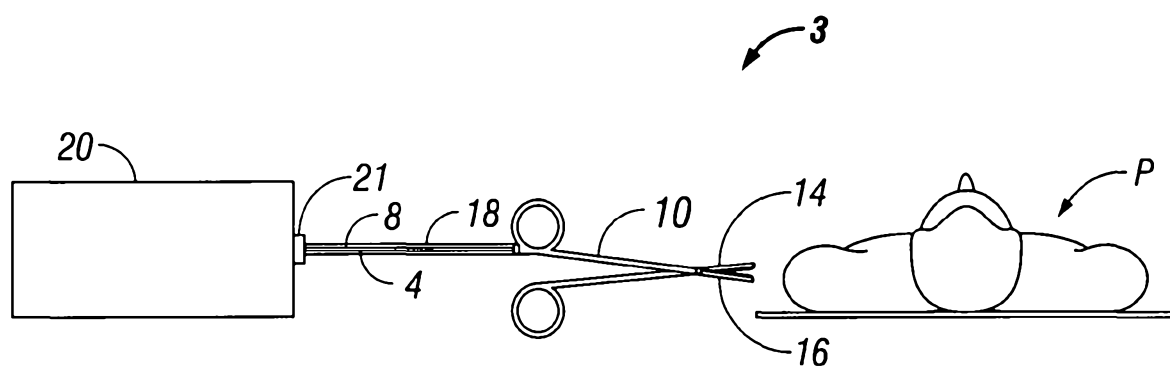


FIG. 1B

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Invention Title:	Crest factor enhancement in electrosurgical generators

The following statement is a full description of this invention, including the best method of performing it known to me/us:

CREST FACTOR ENHANCEMENT IN
ELECTROSURGICAL GENERATORS

CROSS-REFERENCE TO RELATED APPLICATIONS

5 This application claims the benefit of priority to U.S. Provisional Application
Serial No. 61/036,323 entitled "CREST FACTOR ENHANCEMENT IN
ELECTROSURGICAL GENERATORS" filed March 13, 2008 by Robert Behnke et al,
which is incorporated by reference herein. This application also claims the benefit of
10 priority to U.S. Patent Application Serial No. 12/401,981 filed March 11, 2009, which is
incorporated by reference herein.

BACKGROUND

Technical Field

15 The present disclosure relates to electrosurgical apparatuses, systems and
methods. More particularly, the present disclosure is directed to enhancing and/or
maintaining a crest factor of a radiofrequency (RF) waveform in electrosurgical
generators.

Background of Related Art

20 Energy-based tissue treatment is well known in the art. Various types of energy
(e.g., electrical, ultrasonic, microwave, cryo, heat, laser, etc.) are applied to tissue to
achieve a desired result. Electrosurgery involves application of high radio frequency
electrical current to a surgical site to cut, ablate, coagulate or seal tissue. In monopolar
electrosurgery, a source or active electrode delivers radio frequency energy from the

electrosurgical generator to the tissue and a return electrode carries the current back to the generator. In monopolar electrosurgery, the source electrode is typically part of the surgical instrument held by the surgeon and applied to the tissue to be treated. A patient return electrode is placed remotely from the active electrode to carry the current back to the generator.

Ablation is most commonly a monopolar procedure that is particularly useful in the field of cancer treatment, where one or more RF ablation needle electrodes (usually of elongated cylindrical geometry) are inserted into a living body. A typical form of such needle electrodes incorporates an insulated sheath from which an exposed (uninsulated) tip extends. When RF energy is provided between the return electrode and the inserted ablation electrode, RF current flows from the needle electrode through the body. Typically, the current density is very high near the tip of the needle electrode, which tends to heat and destroy surrounding tissue.

In bipolar electrosurgery, one of the electrodes of the hand-held instrument functions as the active electrode and the other as the return electrode. The return electrode is placed in close proximity to the active electrode such that an electrical circuit is formed between the two electrodes (e.g., electrosurgical forceps). In this manner, the applied electrical current is limited to the body tissue positioned between the electrodes. When the electrodes are sufficiently separated from one another, the electrical circuit is open and thus inadvertent contact with body tissue with either of the separated electrodes does not cause current to flow.

It is known in the art that the crest factor of a waveform is a useful measure of the coagulating ability of a radio frequency output. Thus, maintaining a high crest factor would be beneficial in electrosurgical procedures.

SUMMARY

The present disclosure relates to an electrosurgical generator, comprising: a controller configured to generate: a first pulse train including at least one first control pulse and at least one first reset pulse; and a second pulse train including at least one second control pulse and at least one second reset pulse, wherein the at least one first control pulse and the at least one second control pulse are asynchronous and the at least one first reset pulse and the at least one second reset pulse are synchronous; an RF output stage including a first switching element and a second switching element, wherein the at least one first control pulse and the at least one second control pulse are configured to activate the first and second switching elements asynchronously to generate a non-continuous RF waveform, and wherein the at least one first reset pulse and the at least one second reset pulse are configured to synchronously activate the first and second switching elements, respectively, to reset the RF output stage; and a crest factor detection circuit configured to determine a crest factor of the non-continuous RF waveform and adjust at least one property of each of the plurality of the first and second reset pulses based on the crest factor.

A method for performing electrosurgery, the method comprising the steps of: generating a first pulse train, wherein the first pulse train includes at least one first control pulse and at least one first reset pulse; generating a second pulse train, wherein the second pulse train includes at least one second control pulse and at least one second reset pulse, the at least one first control pulse and the at least one second control pulse being asynchronous and the at least one first reset pulse and the at least one second reset pulse being synchronous; supplying the at least one first control pulse train and the at least one second control pulse train to an RF output stage, having a first switching element and a second switching element; activating the first and second switching elements asynchronously to generate a non-continuous RF waveform in response to the plurality of asynchronous first and second control pulses; activating the first and second switching elements synchronously to reset the RF output stage in response to the at least one first reset pulse and at least one second reset pulse; determining a crest factor of the non-continuous RF waveform; and adjusting at least one property of each of the plurality of the first and second reset pulses based on the crest factor.

Another embodiment of the present disclosure includes a method for performing electrosurgery which includes the steps of: setting a desired crest factor for a non-continuous RF waveform; determining an actual crest factor of a non-continuous RF waveform, comparing the desired crest factor with the actual crest factor, and
5 performing an adjustment of a property of a first reset pulse and a property of a second reset pulse to maintain a desired crest factor. The controller is configured to generate a first pulse train having a first control pulse and a first reset pulse. The controller is also configured to generate a second pulse train, having a second control and second reset pulse. The first and second control pulses are asynchronous and the first and second
10 reset pulses are synchronous. Also, the method includes the step of comparing the desired crest factor with the actual crest factor.

BRIEF DESCRIPTION OF THE DRAWINGS

Various embodiments of the present disclosure are described herein with reference to the drawings wherein:

15 FIGS. 1A-1B are schematic block diagrams of an electrosurgical system according to the present disclosure;

FIG. 2 is a schematic block diagram of a generator according to one embodiment of the present disclosure;

FIG. 3 is a schematic diagram of a non-single ended transformer according to
20 the present disclosure;

FIG. 4 is a schematic diagram of a plurality of pulse trains and a 100% duty cycle RF waveform output according to the present disclosure;

FIG. 5 is a schematic diagram of a plurality of pulse trains and a less than 100% duty cycle RF waveform output according to the present disclosure;

FIG. 6 is a graph of a low crest factor RF waveform showing desired and undesired waves according to the present disclosure;

FIG. 7 is a schematic diagram of a plurality of pulse trains and reset pulses and a less than 100% duty cycle RF waveform output according to the present disclosure;

FIG. 8 is a graph of a high crest factor RF waveform showing desired and undesired waves according to the present disclosure;

FIG. 9 is a schematic diagram of a non-single ended transformer according to another embodiment of the present disclosure;

FIG. 10 is a schematic diagram of a plurality of pulse trains according to another embodiment of the present disclosure; and

FIG. 11 is a flow chart of a method of maintaining a crest factor according to the present disclosure.

DETAILED DESCRIPTION

Particular embodiments of the present disclosure are described hereinbelow with reference to the accompanying drawings. In the following description, well-known functions or constructions are not described in detail to avoid obscuring the present disclosure in unnecessary detail.

The electrosurgical generator, according to the present disclosure, can perform monopolar and bipolar electrosurgical procedures, including vessel sealing procedures.

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The generator may include a plurality of outputs for interfacing with various electrosurgical instruments (e.g., a monopolar active electrode, return electrode, bipolar electrosurgical forceps, footswitch, etc.). Further, the generator includes electronic circuitry configured for generating radio frequency power specifically suited for various electrosurgical modes (e.g., cutting, blending, division, etc.) and procedures (e.g., monopolar, bipolar, vessel sealing).

Fig. 1A is a schematic illustration of a monopolar electrosurgical system 1 according to one embodiment of the present disclosure. The system 1 includes an electrosurgical instrument 2 having one or more electrodes for treating tissue of a patient P. The instrument 2 is a monopolar type instrument including one or more active electrodes (e.g., electrosurgical cutting probe, ablation electrode(s), etc.). Electrosurgical RF energy is supplied to the instrument 2 by a generator 20 via an supply line 4, which is connected to an active terminal 30 (Fig. 2) of the generator 20, allowing the instrument 2 to coagulate, seal, ablate and/or otherwise treat tissue. The energy is returned to the generator 20 through a return electrode 6 via a return line 8 at a return terminal 32 (Fig. 2) of the generator 20. The active terminal 30 and the return terminal 32 are connectors configured to interface with plugs (not explicitly shown) of the instrument 2 and the return electrode 6, respectively, which are disposed at the ends of the supply line 4 and the return line 8.

The system 1 may include a plurality of return electrodes 6 that are arranged to minimize the chances of tissue damage by maximizing the overall contact area with the patient P. In addition, the generator 20 and the return electrode 6 may be configured for monitoring so-called "tissue-to-patient" contact to insure that sufficient contact exists therebetween to further minimize chances of tissue damage.

Fig. 1B is a schematic illustration of a bipolar electrosurgical system 3 according to the present disclosure. The system 3 includes a bipolar electrosurgical forceps 10 having one or more electrodes for treating tissue of a patient P. The electrosurgical forceps 10 includes opposing jaw members having an active electrode 14 and a return electrode 16 disposed therein. The active electrode 14 and the return electrode 16 are connected to the generator 20 through cable 18, which includes the supply and return lines 4, 8 coupled to the active and return terminals 30, 32, respectively (Fig. 2). The electrosurgical forceps 10 is coupled to the generator 20 at a connector 21 having connections to the active and return terminals 30 and 32 (e.g., pins) via a plug disposed at the end of the cable 18, wherein the plug includes contacts from the supply and return lines 4, 8.

The generator 20 includes suitable input controls (e.g., buttons, activators, switches, touch screen, etc.) for controlling the generator 20. In addition, the generator 20 may include one or more display screens for providing the user with variety of output information (e.g., intensity settings, treatment complete indicators, etc.). The controls allow the user to adjust power of the RF energy, waveform, and other parameters to achieve the desired waveform suitable for a particular task (e.g., coagulating, tissue sealing, intensity setting, etc.). The instrument 2 may also include a plurality of input controls that may be redundant with certain input controls of the generator 20. Placing the input controls at the instrument 2 allows for easier and faster modification of RF energy parameters during the surgical procedure without requiring interaction with the generator 20.

FIG. 2 illustrates a schematic block diagram of the generator 20 according to one embodiment of the present disclosure. The generator 20 includes a controller 24, a high

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voltage DC power supply 27 (HVPS) and an RF output stage 28. The controller 24 includes a power supply (not shown), for example, a low voltage DC power supply, which provides low voltage power to circuitry of the controller 24 and/or RF output stage 28. The HVPS 27 is connected to a conventional AC source (e.g., electrical wall outlet) and provides high voltage DC power to an RF output stage 28, which then converts high voltage DC power into RF energy and delivers the RF energy to the active terminal 30. The energy is returned thereto via the return terminal 32.

In particular, the RF output stage 28 generates sinusoidal waveforms of high RF energy. The RF output stage 28 is configured to generate a plurality of waveforms having various duty cycles, peak voltages, crest factors, and other suitable parameters. Certain types of waveforms are suitable for specific electrosurgical modes. For instance, the RF output stage 28 generates a 100% duty cycle sinusoidal waveform in cut mode, which is best suited for ablating, fusing and dissecting tissue and a 1-25% duty cycle waveform in coagulation mode, which is best used for cauterizing tissue to stop bleeding.

The generator 20 may include a plurality of connectors to accommodate various types of electrosurgical instruments (e.g., instrument 2, electrosurgical forceps 10, etc.). Further, the generator 20 is configured to operate in a variety of modes such as ablation, monopolar and bipolar cutting coagulation, etc. It is envisioned that the generator 20 may include a switching mechanism (e.g., relays) to switch the supply of RF energy between the connectors, such that, for instance, when the instrument 2 is connected to the generator 20, only the monopolar plug receives RF energy.

The controller 24 includes a microprocessor 25 operably connected to a memory 26, which may be volatile type memory (e.g., RAM) and/or non-volatile type memory

(e.g., flash media, disk media, etc.). The microprocessor 25 includes an output port that is operably connected to the HVPS 27 and/or RF output stage 28 allowing the microprocessor 25 to control the output of the generator 20 according to either open and/or closed control loop schemes. Those skilled in the art will appreciate that the microprocessor 25 may be substituted by any logic processor (e.g., control circuit) adapted to perform the calculations discussed herein.

A closed loop control scheme is a feedback control loop wherein sensor circuit 22 and/or crest factor detection circuit 23, which both may include a plurality of sensors measuring a variety of tissue and energy properties (e.g., tissue impedance, tissue temperature, output current and/or voltage, crest factor, etc.), provide feedback to the controller 24. Such sensors are within the purview of those skilled in the art. The controller 24 then signals the HVPS 27 and/or RF output stage 28, which then adjust DC and/or RF power supply, respectively. The controller 24 also receives input signals from the input controls of the generator 20 or the instrument 2. The controller 24 utilizes the input signals to adjust power outputted by the generator 20 and/or performs other control functions thereon.

FIG. 3 depicts a schematic diagram of the RF output stage 28 having a transformer 40. In one embodiment, transformer 40 is a non-single ended transformer, configured in a simplified push-pull topology. It is also envisioned the present system and method may be applied to any non-single ended transformer topology (e.g., full bridge) having a primary winding 41 and secondary winding 43. The primary winding 41 is coupled to the HVPS 27 and includes a first switching element 42 and a second switching element 44 which may be, for example, transistors, FETs, MOSFETs or the like. The switching elements 42 and 44 are coupled to the controller 24 which controls

the operation thereof to generate RF energy. More specifically, the controller 24 is configured to transmit a low-voltage clock signal of a first pulse train 60 to switching element 42 and a second pulse train 62 to switching element 44 of the RF output stage 28 (shown in FIG. 6). The secondary winding 43 is coupled to the active terminal 30 and return terminal 32.

In various types of control loops it may be desirable to measure certain properties of RF energy being delivered by the RF output stage 28. In particular, voltage is continuously measured and impedance is calculated by the sensor circuit 22. In one embodiment, a control loop may be configured to measure the crest factor of a waveform and maintain the crest factor at a desired level. Crest factor is a useful measurement of the coagulation ability of an RF output waveform, thus increasing or controlling the crest factor is beneficial to electrosurgical procedures involving coagulation.

The present disclosure provides a system and method for maintaining a desired crest factor of an RF waveform. A high crest factor waveform is particularly helpful in electrosurgical procedures. The crest factor is defined as the ratio of the peak voltage and root mean square (RMS) voltage for symmetrical waveforms, those having a 100% duty cycle (e.g., when there is no interruption or pause in the RF waveform).

$$(1) CF = V_{PEAK} / V_{RMS}$$

For non-symmetrical waveforms, the crest factor is defined as the ratio of peak to peak voltage and twice the RMS voltage.

$$(2) CF = V_{(PEAK-PEAK)} / 2 * V_{RMS}$$

Electrosurgical generators have difficulties generating high crest factor waveforms primarily due to excessive ringing, during the off-time or pause stage. The ringing in the RF waveform is especially excessive in high impedance loads. This occurs due to an increase in the RMS of the waveform and which decreases the crest factor, as seen in the above formula (2). When the undesired ringing is removed, the RMS of the waveform is decreased, thus increasing the crest factor (e.g., maintaining the crest factor).

FIG. 4 illustrates a schematic diagram of a plurality of pulse trains and a corresponding 100% duty cycle RF waveform. As mentioned above, the controller 24 is configured to transmit a low-voltage clock signal sourced from the low-voltage power supply (not shown), as a first pulse train 60 to switching element 42 and a second pulse train 62 to switching element 44 of the RF output stage 28. Each of the pulse trains includes a plurality of control pulses 60a and 62a, respectively. When a 100% duty cycle waveform is desired, i.e., when there is no pause or interruption in power (shown in output wave 64 in FIG. 4), the first and second control pulse trains 60a and 62a are non- synchronous and continuous. The RF waveform 64 is generated as the first pulse train 60 and the second pulse train 62 to control the respective switching elements 40 and 42.

More specifically, the first pulse train 60 activates the pull of the RF output stage 28 when the square wave of the clock signal is at its highest amplitude, namely when the first control pulse 60a activates the switching element 42. The second pulse train 62 activates the push of the RF output stage 28 when the square wave of the clock signal is at its highest amplitude, such that the second control pulse 62a activates the switching element 44. By alternating the first and second control pulses 60a and 62a

and spacing the control pulses 60a and 62a at $\frac{1}{2}$ cycle timing (e.g., 180° out of phase), the RF waveform 64 is created at a specified frequency. Further, tuning can be done with inductors and capacitors and/or the parasitics of the transformer 40 to give a sinusoidal output as illustrated in output wave 64 in FIG. 4.

FIG. 5 depicts a schematic diagram of a plurality of pulse trains and a less than 100% duty cycle RF waveform output. The waveform 64 has a duty cycle of less than 100%. The first and second control pulses 60a and 62a are out of phase by 180° . In other words, the pulses are staggered, which allows for generation of non-synchronous waveforms. Further, there is a period of time when both the first and second control pulses 60a and 62a are paused to provide for off-time of the waveform. Ringing occurs in a region 66 when the first and second control pulse trains 60a and 62b are paused during the RF waveform off time, hence less than 100% duty cycle.

The region 66 shows the RF waveform 64 decaying steadily due to a pause in pulse trains 60 and 62, i.e., no activity. The region 66 is defined as the region where switching elements 42 and 44 (shown in FIG. 3) do not receive the pulse trains 60 and 62 from the controller 24. Although there is a pause in the pulse trains 60 and 62, there is still sufficient energy stored in the tuning elements of the transformer 40, thus energy rings out. When the control pulse trains 60 and 62 are stopped in the RF output stage 28, ringing occurs in the region 66 of the waveform 64, since stored energy still exists in the circuitry. The ringing in the region 66, in turn, reduces the crest factor in the RF waveform 64, as illustrated in FIG. 5. In order to maintain a high crest factor waveform output of the electrosurgical unit, the ringing in the waveform 64, shown in region 66 must be decreased and/or eliminated.

FIG. 6 illustrates the effect of ringing on non-synchronous waveforms with less than 100% duty cycle. FIG. 6 shows a graph of a low crest factor RF waveform 50 showing desired and undesired waves according to the present disclosure. The low crest factor waveform 50 includes desired waves 52 and 54 and an excessive ringing wave region 60. The excessive ringing propagates from an undesired wave 56 to a smaller undesired wave 58, with gradually decreasing sized waves. The RMS of the waveform 50 is increased due to excessive ringing, thus decreasing the crest factor.

FIG. 7 depicts a schematic diagram of a plurality of pulse trains and reset pulses adapted to generate a less than 100% duty cycle RF waveform output, according to the present disclosure. To maintain a high crest factor, the first and second pulse trains 60 and 62 include, in addition to the first and second control pulse 60a and 62a, a first and second reset pulses 60b and 62b which are transmitted synchronously and simultaneously (e.g., in phase) to the switching elements 42 and 44. The reset pulses are preferably of substantially the same duration. When the first and second reset pulses 60b and 62b are synchronously and simultaneously transmitted by the controller 24, the non-continuous RF waveform 64 generates substantially no ringing. Namely, the controller 24 is short-circuiting the RF output stage at the switching elements 42 and 44 by transmitting first and second reset pulses 60b and 62b simultaneously. The substantial decrease in ringing is depicted at 64b of the waveform 64 in region 68 due to short-circuiting of the RF output stage 28.

It is envisioned that the timing of the first and second reset pulses 60b and 62b may be adjusted depending on the patient load and/or different electrosurgical procedure. For example, the start time of first and second reset pulse 60b and 62b transmitted by the controller 24 may vary. It is also envisioned that the duration of the

first and second reset pulses 60b and 62b may vary in different electrosurgical procedures and/or different patients. All of these required and/or desired adjustments may be made by the controller 24 by transmitting the clock signal to the switching elements.

5 In embodiments, the desired crest factor can be adjusted in real-time based on certain parameters, for example, but not limited to, tissue impedance, duration of time since activation time T_n , repeating pattern(s), tissue temperature, and blade temperature. These parameters may be adjusted by the controller or by a user.

10 In other embodiments, the crest factor can be adjusted by changing the duty cycle, e.g., the number of pulses, of pulse patterns. More particularly, the pulse pattern may be adjusted to a single pulse pattern (i.e., spray coagulation mode), having a duty cycle of about 4.6%, to a multi-pulse pattern (i.e., blend mode or pure cut mode), having a duty cycle of about 100%. By adjusting the duty cycle from about 4.6% to about 100%, this, in turn, adjusts the crest factor from about 1.4 to about 8.0.

15 FIG. 8 illustrates a graph of a high crest factor RF waveform 50' showing desired and undesired waves according to the present disclosure. The high crest factor waveform 50' includes desired waves 52' and 54'. The high crest factor waveform 50' also includes an excess ringing wave region 60'. The excessive ringing is reduced and propagates between undesired waves 56' and 58'. The reduction in the ringing is seen
20 in the undesired waves 56', 58' being substantially similar in size. Unlike the excessive ringing wave region 60, the waves of region 60' are also substantially smaller. In this scenario, the RMS of the waveform 50' is decreased, since the undesired ringing waves 56' and 58' are small, thus increasing the crest factor.

FIG. 9 and 10 illustrate another embodiment of present disclosure. FIG. 9 is a schematic diagram of the RF output stage 28 according to another embodiment of the present disclosure. The RF output stage 28 includes a non-single ended transformer 40 configured in a simplified push-pull topology. Transformer 40 includes a switching element 42, a switching element 44 and a switching element 48. The switching element 48 is coupled in series to a resistive load 49. In addition to transmitting a clock frequency of a first pulse train 60 and a second pulse train 62 to the switching elements 42 and 44 of the RF output stage 27, respectively, the controller 24 also transmits a third pulse train 63 to the switching element 48.

FIG. 10 illustrates a schematic diagram of a plurality of pulse trains transmitted by the controller 24. The third control pulse lasts a period which is substantially for the duration of the off-time of the switching elements 42 and 44, such that during the off-time at switching elements 42 and 44, the switching element 48 is activated. As a result, the energy out of the transformer 40 and all of the inductors and capacitors and/or the parasitics of the transformer 40 is dumped into the resistive load 49. During the activation of the switching element 48, the RF waveform 64 shows substantially no ringing at region 69 since all the energy was dumped into the resistive load 49. The substantial decrease in ringing is depicted at 64b of the waveform 64 in region 69. Therefore, the crest factor of RF waveform 64 is maintained and/or increased, thus aiding in coagulation in electrosurgical procedures.

FIG. 11 shows a flow chart of a method for maintaining a desired crest factor according to the present disclosure. The method utilizes a crest factor detection circuit 23 which can be implemented in a closed loop control scheme as part of the sensor circuit 22. As mentioned above, to maintain the desired crest factor of the RF

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waveform 64, excessive ringing must be minimized. In step 100, a desired crest factor is selected and set on the generator 20. A user may manually set the desired crest factor on the generator 20 or the desired crest factor may be automatically set by the generator 20. It is envisioned that the automatic determination of the desired crest factor of generator 20 may depend on any other inputs entered by the user and/or other parameters. Some of the parameters may be, for example, but not limited to, tissue impedance, duration of time since activation time T_n , tissue temperature, and/or a time varying pattern. The desired crest factor may be a value that is selected for a specific electrosurgical procedure and/or a value that is associated with a certain electrosurgical instrument.

In step 102, the crest factor detection circuit 23 calculates and determines an actual crest factor of the non-continuous RF waveform 64 (FIG. 7). The crest factor detection circuit 23 measures the voltage and calculates the peak and RMS voltage based on the above-discussed formulas (1) and (2). The voltage values are then used by the crest factor detection circuit 23 to determine the crest factor.

In other embodiments, the crest factor detection circuit 23 may be configured to calculate and determine an actual "current" crest factor of a "current" waveform (not shown). The "current" crest factor is defined as the ratio of peak current and the RMS current.

$$(3) ICF = I_{PEAK} / I_{RMS}$$

The current values are then used by the crest factor detection circuit 23 (similarly to the RF waveform crest factor) to determine the "current" crest factor.

In step 104, the microprocessor 25 and/or the crest factor detection circuit 23 compares the actual crest factor with the desired crest factor, thereby determining a crest factor error. The controller 24 determines if the actual crest factor is lower or higher than the desired crest factor. If the desired crest factor is less than or greater than the actual crest factor, the method proceeds to step 106, in which the properties of the first and second reset pulses 60b and 62b (FIG. 7) are adjusted by the controller 24 in order to decrease or increase the actual crest factor in order to match the desired crest factor. For example, frequency, period, duty cycle and other properties of the first and second reset pulses 60b and 62b may be adjusted.

According to one embodiment of the present disclosure, an activation time T_n+a (e.g., duty cycle) and a duration time T_m (e.g., period of the pulse) of the synchronous reset pulses 60b and 62b may be varied. In particular, the duty cycle of the first and second reset pulses 60b and 62b transmitted by the controller 24 may be varied by adjusting the off-time period, T_n+a , wherein T_n is the time period or remaining portion of the control pulse 62a, and wherein a is the time period between the trailing control pulse (e.g., control pulse 62a) and the first and second reset pulses 60b and 62b. As shown in FIG. 7, the on-time period, T_m , between the synchronous reset pulses 60b and 62b may also be adjusted. Some of the factors that may determine the variation of the activation time T_n+a and the duration time T_m of the first and second reset pulses 60a and 60b are the tissue composition of the patient, the user's treatment plan, and/or the effect on certain parameters of the waveform (e.g., crest factor, wave length, wave period, etc.).

Afterwards, the method loops back to step 100 and repeats the steps of maintaining a desired crest factor. It is also envisioned that an additional step may be

included to scan the actual RF waveform for ringing beyond the specified duty cycle.

As a result of the scan, the RF waveform may be analyzed to determine when the following synchronous reset pulses and/or the control pulses may be activated.

While several embodiments of the disclosure have been shown in the drawings and/or discussed herein, it is not intended that the disclosure be limited thereto, as it is intended that the disclosure be as broad in scope as the art will allow and that the specification be read likewise. Therefore, the above description should not be construed as limiting, but merely as exemplifications of particular embodiments. Those skilled in the art will envision other modifications within the scope and spirit of the claims appended hereto.

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CLAIMS:

1. An electrosurgical generator, comprising:

a controller configured to generate:

a first pulse train including at least one first control pulse and at least one first reset pulse; and

a second pulse train including at least one second control pulse and at least one second reset pulse, wherein the at least one first control pulse and the at least one second control pulse are asynchronous and the at least one first reset pulse and the at least one second reset pulse are synchronous;

an RF output stage including a first switching element and a second switching element, wherein the at least one first control pulse and the at least one second control pulse are configured to activate the first and second switching elements asynchronously to generate a non-continuous RF waveform, and wherein the at least one first reset pulse and the at least one second reset pulse are configured to synchronously activate the first and second switching elements, respectively, to reset the RF output stage; and

a crest factor detection circuit configured to determine a crest factor of the non-continuous RF waveform and adjust at least one property of each of the plurality of the first and second reset pulses based on the crest factor.
2. An electrosurgical generator according to claim 1, wherein the at least one first reset pulse follows the at least one first control pulse and the at least one second reset pulse follows the at least one second control pulse.
3. An electrosurgical generator according to claim 1, wherein the at least one property is selected from the group consisting of a pulse width, a frequency and a duty cycle.
4. An electrosurgical generator according to claim 1, wherein the RF output stage further includes a non-single ended transformer.
5. An electrosurgical generator according to claim 4, wherein the transformer is

configured in a full-bridge topology.

6. An electrosurgical generator according to claim 4, wherein the transformer is configured in a push-pull topology.
7. An electrosurgical generator according to claim 4, wherein the transformer includes a primary winding and a secondary winding, the primary winding including the first and second switching elements.
8. An electrosurgical generator according to claim 7, wherein the primary winding further includes a third switching element coupled to a resistive load.
9. An electrosurgical generator according to claim 8, wherein the controller is configured to generate a third pulse train including a third control pulse, the third control pulse being configured to activate the third switching element during an off-time of the first and second switching elements to dump remaining energy stored in the RF output stage.
10. A method for performing electrosurgery, the method comprising the steps of:
 - generating a first pulse train, wherein the first pulse train includes at least one first control pulse and at least one first reset pulse;
 - generating a second pulse train, wherein the second pulse train includes at least one second control pulse and at least one second reset pulse, the at least one first control pulse and the at least one second control pulse being asynchronous and the at least one first reset pulse and the at least one second reset pulse being synchronous;
 - supplying the at least one first control pulse train and the at least one second control pulse train to an RF output stage, having a first switching element and a second switching element;
 - activating the first and second switching elements asynchronously to generate a non-continuous RF waveform in response to the plurality of asynchronous first and second control pulses;

activating the first and second switching elements synchronously to reset the RF output stage in response to the at least one first reset pulse and at least one second reset pulse;

determining a crest factor of the non-continuous RF waveform; and

adjusting at least one property of each of the plurality of the first and second reset pulses based on the crest factor.

11. A method of performing electrosurgery according to claim 10, wherein the at least one property is selected from the group consisting of a pulse width, a frequency and a duty cycle.

12. A method of performing electrosurgery according to claim 11, further comprising the step of:

generating a third pulse train including a third control pulse for controlling a third switching element.

13. A method of performing electrosurgery according to claim 12, further comprising the step of:

activating the third switching element during an off-time of the first and second switching elements to dump remaining energy stored in the RF output stage.

14. An electrosurgical generator substantially as described herein with reference to the accompanying drawings.

15. A method for performing electrosurgery, the method being substantially as described herein with reference to the accompanying drawings.

Covidien LP

Patent Attorneys for the Applicant

SPRUSON & FERGUSON

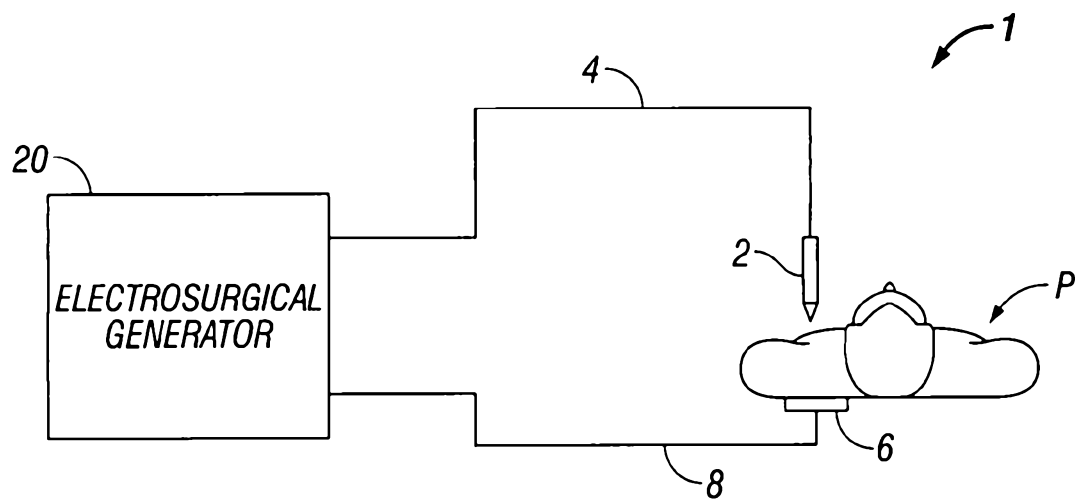


FIG. 1A

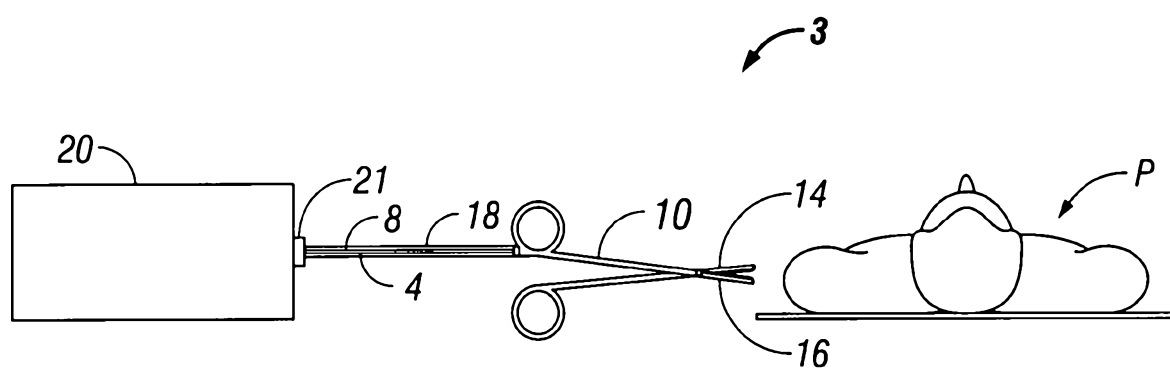


FIG. 1B

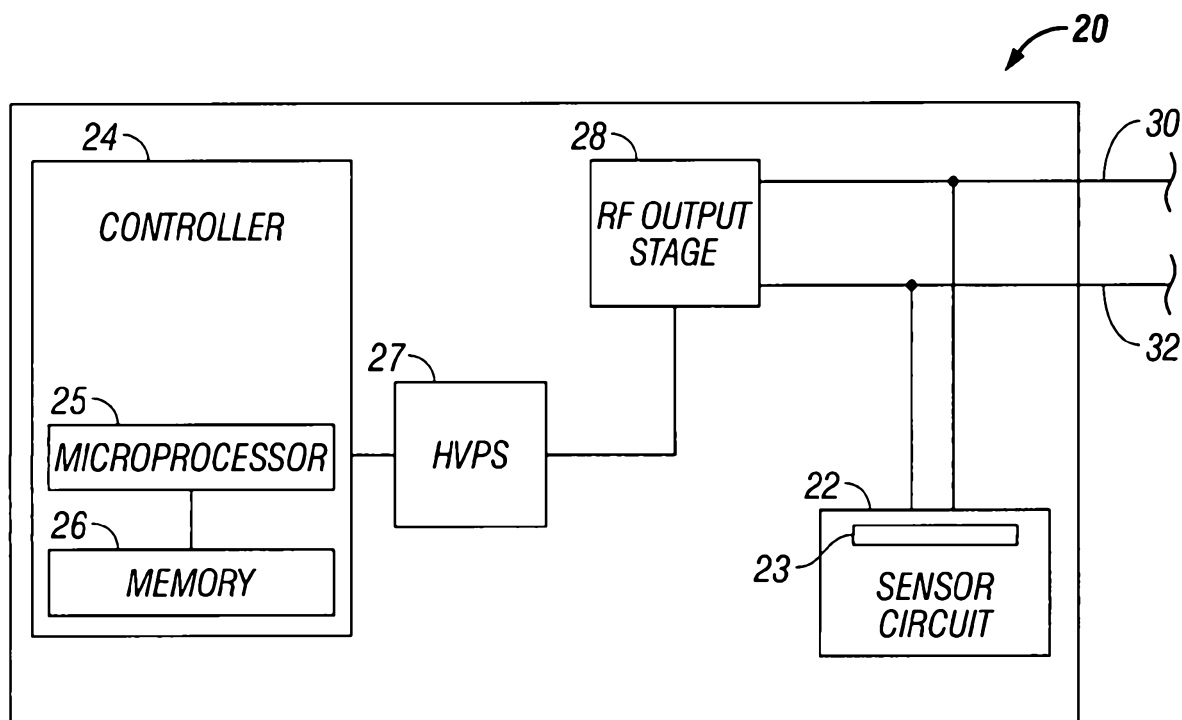


FIG. 2

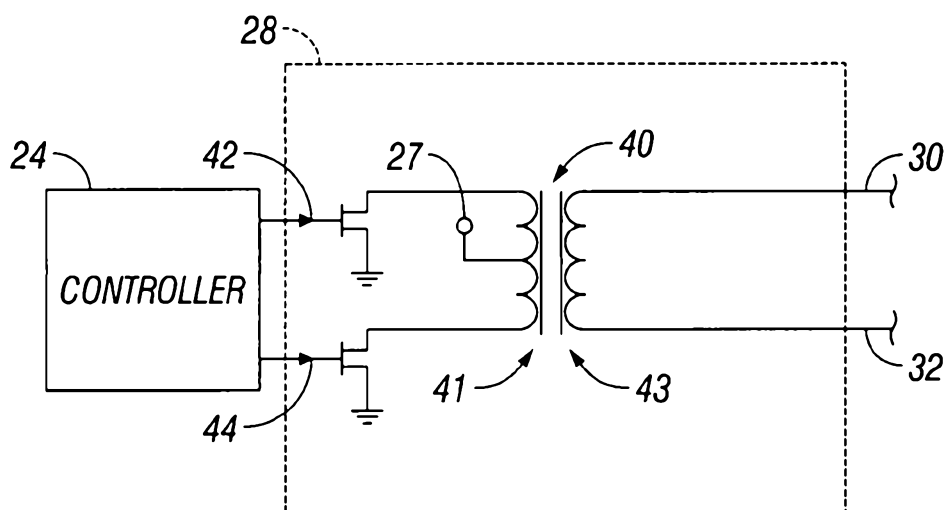


FIG. 3

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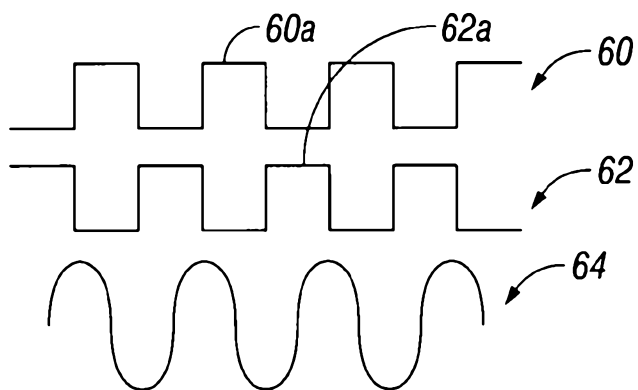


FIG. 4

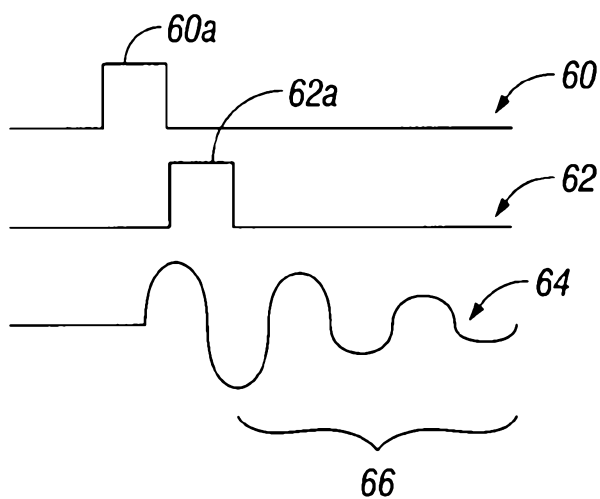


FIG. 5

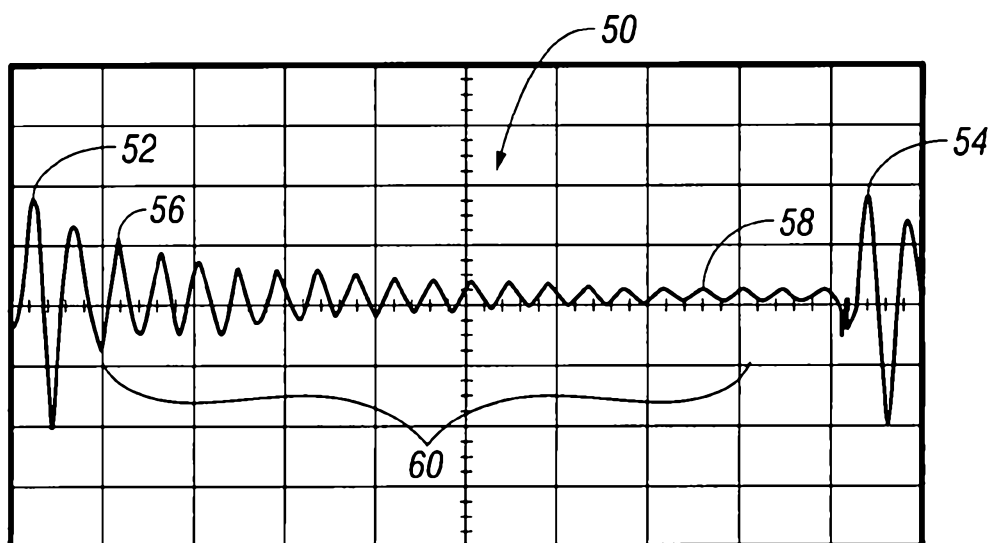


FIG. 6

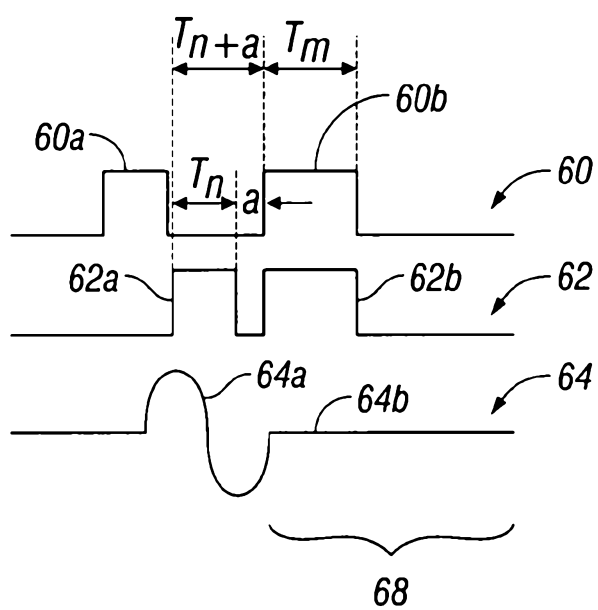


FIG. 7

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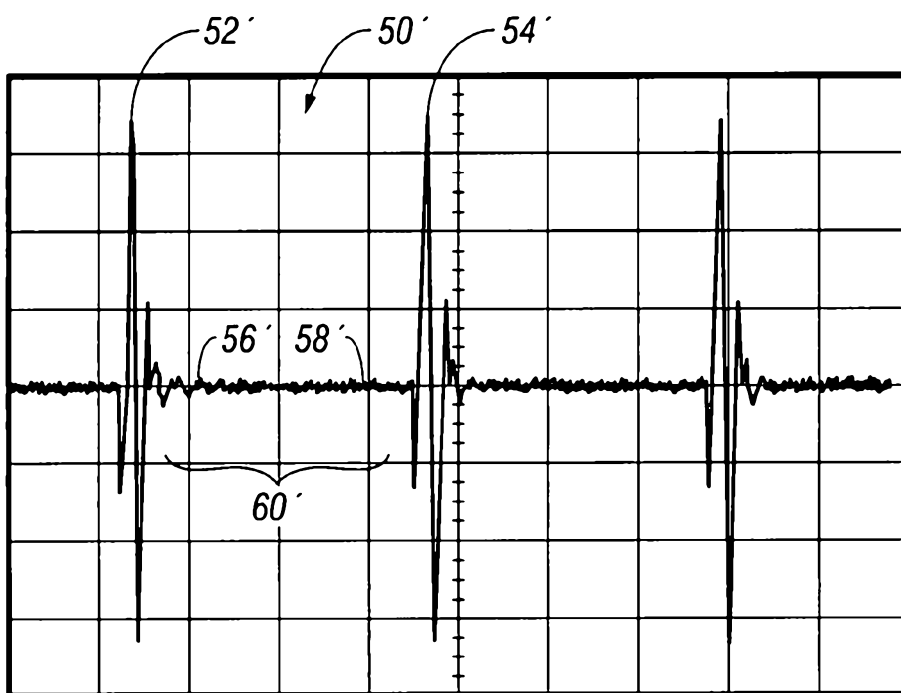


FIG. 8

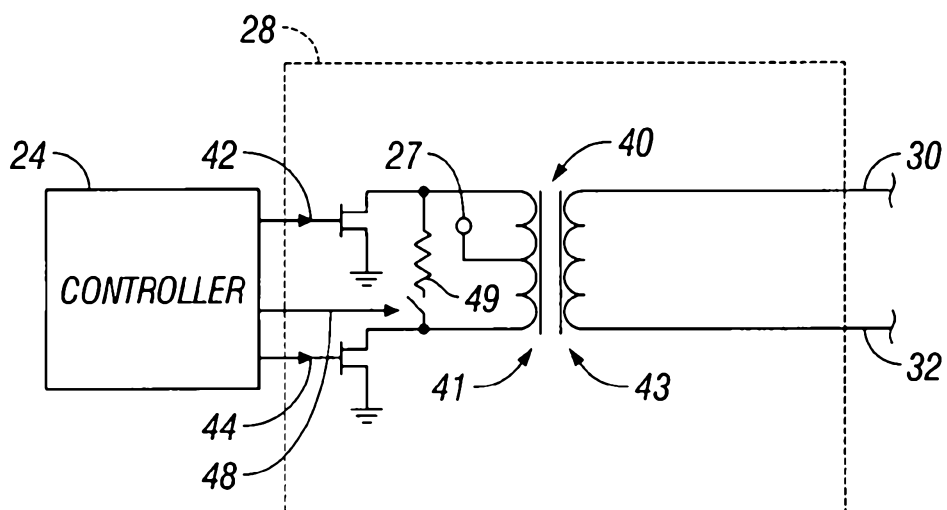


FIG. 9

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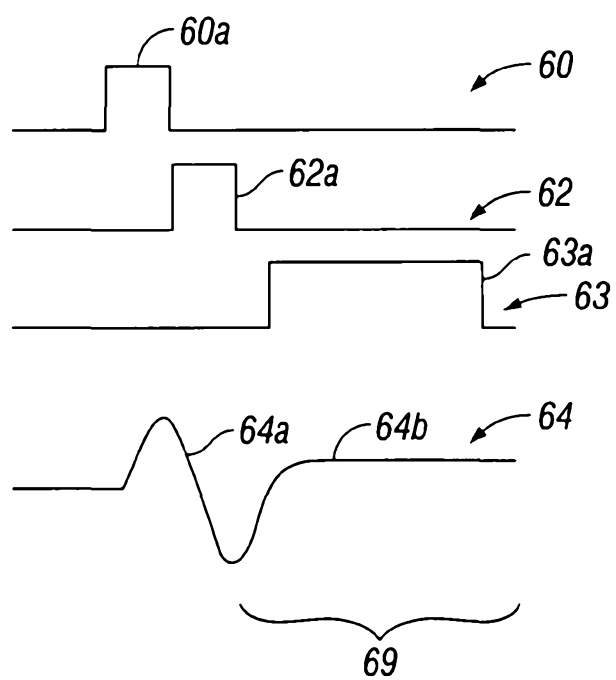


FIG. 10

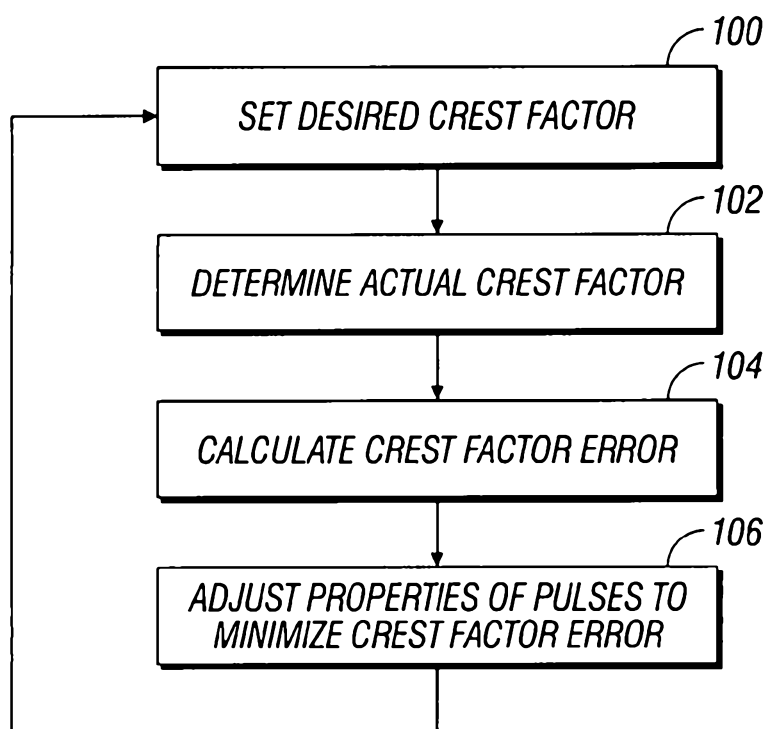


FIG. 11