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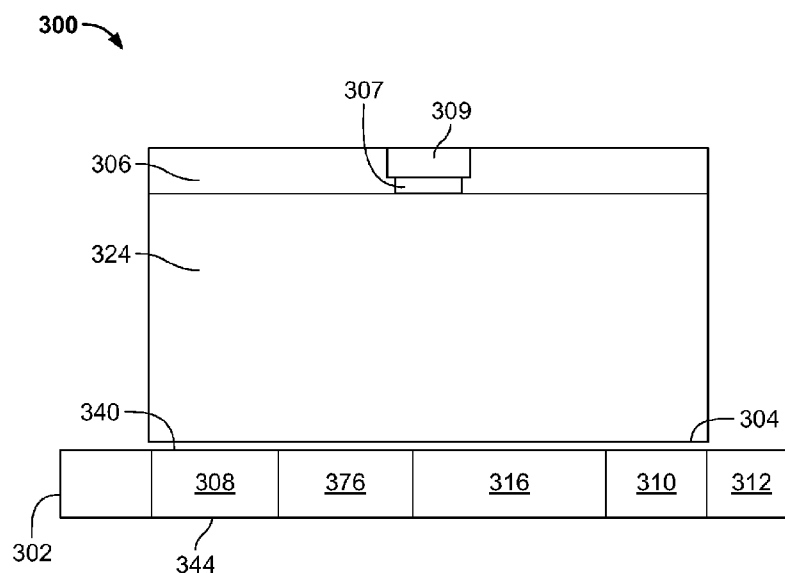


FIG. 3A

(57) Abstract: The present specification provides a dialysate management system for generating, weighing, and heating a dialysate fluid during a dialysis treatment. The dialysate management system includes a container and base enclosure. A bottom surface of the container rests within the base enclosure, which is configured to weigh the fluid in the container and measure its conductivity. The fluid may be heated using a heater integrated into the base enclosure or positioned in-line with a fluid pathway. The base of the container is preferably sloped and positioned within the internal volume of the container is a disposable prescription bag having a predefined quantity of prescription compositions that dissolve when water is poured into the container.



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METHODS AND SYSTEMS FOR MEASURING AND HEATING DIALYSATE**CROSS-REFERENCE TO RELATED APPLICATIONS**

The present application relies on United States Patent Application Number 15/482,620,
5 entitled “Methods and Systems for Measuring and Heating Dialysate” and filed on April 7, 2017,
for priority.

The present application also relates to the following applications, all of which are herein
incorporated by reference in their entirety:

U.S. Patent Application No. 15/447,519, entitled “Split Reservoir Bags and Method of
10 Using Split Reservoir Bags to Improve the Heating and Generation of Dialysate” and filed on
March 2, 2017.

U.S. Patent Application No. 14/924,134, entitled “Method and System of Monitoring
Electrolyte Levels and Composition Using Capacitance or Induction” and filed on October 27,
2015, which is a continuation application of U.S. Patent Application No. 13/725,178, of the same
15 title, filed on December 21, 2012, and issued as U.S. Patent No. 9,201,036 on December 1, 2015.
U.S. Patent Application No. 14/848,012, entitled “Load Suspension and Weighing System for a
Dialysis Machine Reservoir” and filed on September 8, 2015, which is a continuation application
of U.S. Patent Application No. 13/726,450, of the same title, filed on December 24, 2012, and
issued as U.S. Patent No. 9,157,786 on October 13, 2015.

20 U.S. Patent Application No. 15/055,857, entitled “Manifold Diaphragms” and filed on
February 29, 2016, which is a continuation application of U.S. Patent Application No.
13/852,918, of the same title, filed on March 28, 2013, and issued as U.S. Patent No. 9,308,307
on April 12, 2016, which is a continuation-in-part application of U.S. Patent Application No.
13/023,490, entitled “Portable Dialysis Machine”, filed on February 8, 2011, and issued as U.S.
25 Patent No. 8,597,505 on December 3, 2013;

U.S. Patent Application No. 15/147,639, entitled “Portable Dialysis Machine with
Improved Reservoir Heating System” and filed on May 5, 2016, which is a continuation
application of U.S. Patent Application No. 13/726,457, of the same title, filed on December 24,
2012, and issued as U.S. Patent No. 9,358,331 on June 7, 2016, which is a continuation-in-part
30 application of U.S. Patent Application No. 13/023,490, entitled “Portable Dialysis Machine”,
filed on February 8, 2011, and issued as U.S. Patent No. 8,597,505 on December 3, 2013;

U.S. Patent Application No. 15/341,953, entitled “Portable Dialysis Machine” and filed on November 2, 2016, which is a continuation application of U.S. Patent Application No. 14/040,362, of the same title, filed on September 27, 2013, and issued as United States Patent No. 9,517,296 on December 13, 2016, which is a continuation application of U.S. Patent Application
5 No. 13/023,490, of the same title, filed on February 8, 2011, and issued as U.S. Patent No. 8,597,505 on December 3, 2013.

FIELD

10 The present specification is directed to dialysis systems with improved structural and functional features. In particular, the present specification is directed to a dialysate management system for holding, heating and measuring dialysate.

BACKGROUND

15 Blood purification systems, which are used for conducting hemodialysis, hemodiafiltration or hemofiltration, involve the extracorporeal circulation of blood through an exchanger with a semi-permeable membrane. Such systems further include fluid circuits for circulating blood, replacement fluid, and/or dialysate including certain electrolytes in concentrations approximating the blood of a healthy person.

20 Hemodialysis (“HD”), using a high flux membrane, removes toxins from the blood using transport mechanisms including diffusion and ultrafiltration (i.e., convective transport). Diffusion removes toxins using a concentration gradient across the semi-permeable membrane. For example, in a hemodialysis circuit, the dialysate solution flows on one side of the dialyzer membrane in one direction while simultaneously blood flows on the other side of the membrane. Ultrafiltration occurs when water (along with small solutes) is driven from the blood to dialysate
25 in the dialyzer because of the hydrostatic pressure gradient between the blood and dialysate compartments (i.e., the transmembrane pressure (“TMP”)).

Conventionally, a reservoir bag is provided for storing the dialysate. The dialysate, which is typically made of filtered water mixed with certain prescribed compositions, is heated to a predefined temperature, namely the patient’s body temperature, before being implemented in
30 a hemodialysis treatment. For example, a clinician may take a 10-liter jug, fill it with 6 liters of water, mix in powdered forms of the prescribed compositions, and then shake the combination to

mix the water and compositions. A sample of the mixture is then taken extracted from the bag and subjected to a conductivity and/or concentration measurement, which is inputted into the dialysis machine. The bag is connected to the dialysate circuit of the dialysis system and the dialysate solution is then pumped through a sorbent cartridge to filter it. Once passed through
5 the sorbent, the filtered dialysate passes into a reservoir where it is subsequently heated.

There are several disadvantages with this conventional system. First, in a standard dialysis treatment, it takes too long to generate filtered, heated dialysate. The priming time requires first waiting for all of the dialysate mixture to pass through a sorbent cartridge and then waiting for all of the filtered dialysate to heat to a predefined temperature, e.g. 37°C. This serial
10 approach to creating filtered, heated dialysate unnecessarily extends patient treatment times and increases patient discomfort.

Second, in conventional systems, operators often forget where they are in the dialysate generation process. Consequently, many lose track as to whether they filled the reservoir with the right amount of water, added in each one of the required compositions, and/or added in the
15 right amount of each composition. As a result, dialysis treatments often have to be restarted in order to ensure the right dialysate mixture is being used.

Hence, there is need for a dialysate management system, and accompanying methods of use, which enable filtered, heated dialysate to be generated without having to serially filter and then heat the dialysate. There is also need for a dialysate container that is physically separate and
20 distinct from the dialysis system and that is configured to determine the conductivity and weight of any solution contained therein, thereby allowing for the elimination of weight measurement and/or conductivity elements from the dialysis machine. There is also a need for dialysate containers, and accompanying methods of use, which reduce the overall number of steps in a conventional dialysis treatment and, hence, also reduce the time required in preparing a dialysis
25 system for performing dialysis.

SUMMARY

In some implementations, the present specification discloses a dialysate generation system for generating a dialysate fluid during a dialysis treatment, comprising: a container configured to
30 hold fluid, wherein the container comprises an internal base surface that, relative to a substantially horizontal surface, has a slope in a range of 0.1 degrees to 50 degrees and an outlet

tube that is in fluidic communication with a fluid circuit of a dialysis system; and a base enclosure configured to detachably receive a bottom portion of the container, wherein said base enclosure comprises: a first scale in physical communication with the bottom portion of the container and configured to weigh the fluid positioned within the container; and a conductivity sensor positioned proximate the bottom portion of the container and configured to measure a conductivity of the fluid in the container.

Optionally, the container further comprises powdered compositions enclosed within a disposable porous material.

Optionally, the outlet tube is positioned proximate to a lowest point of said sloped internal base surface and opposite from the highest point of said sloped internal base surface.

Optionally, said outlet tube is positioned at a height ranging from $\frac{1}{4}$ to $\frac{1}{2}$ inch from an external bottom surface of said container.

Optionally, the dialysate generation system further comprises a wireless transmitter configured to wirelessly transmit at least one of weight data and conductivity data to a controller in a dialysis machine, wherein said dialysis machine is in electronic communication with said dialysate generation system.

Optionally, the first scale comprises a flexure assembly. Optionally, the flexure assembly comprises at least one of a load cell or strain gauge.

Optionally, the conductivity sensor comprises a conductivity coil.

Optionally, the conductivity sensor comprises ultrasonic sensors.

Optionally, the base enclosure and container are physically separate from the dialysis system and wherein the container and base lack a heating element.

In some implementations, the present specification describes a dialysis system, comprising: a dialysis machine comprising: a dialysate fluid circuit having a fluid pathway and a blood fluid circuit, a dialyzer in fluid communication with the dialysate fluid circuit and blood fluid circuit, a sorbent cartridge in fluid communication with said dialysate fluid circuit, a plurality of pumps in physical communication with the dialysate fluid circuit and the blood fluid circuit, a processing unit for controlling an operation of the plurality of pumps, and a heating element configured to heat fluid as it flows through the fluid pathway; and a dialysate generation system physically separate from said controller unit, the dialysate generation system comprising: a container configured to hold fluid, wherein the container comprises an outlet tube that is in fluid

communication with said fluid pathway in the dialysate fluid circuit, a bottom portion, and an internal base surface, and a base enclosure configured to detachably receive the bottom portion of the container, wherein said base enclosure comprises: a scale in physical communication with the bottom portion of the container and configured to weigh the fluid positioned within the
5 container; and a conductivity sensor configured to measure a conductivity of the fluid in the container.

Optionally, the heating element is a resistive heating element positioned longitudinally along and cylindrically around said fluid pathway.

Optionally, the heating element is an inductive heating element positioned longitudinally
10 along and cylindrically around said fluid pathway.

Optionally, the container comprises an internal base surface that, relative to a substantially horizontal surface, has a slope in a range of 0.1 degrees to 50 degrees.

Optionally, the outlet tube is positioned proximate to a lowest point of said sloped internal base surface and opposite from the highest point of said sloped internal base surface.

Optionally, the outlet tube is positioned at a height ranging from $\frac{1}{4}$ to $\frac{1}{2}$ inch from an
15 external bottom surface of said container.

Optionally, the container further comprises powdered compositions enclosed within a disposable porous material.

Optionally, the dialysate generation system further comprises a wireless transmitter
20 configured to wirelessly transmit at least one of weight data and conductivity data to the processing unit.

In some implementations, the present specification discloses a method of generating dialysate using a dialysate generation system, wherein said dialysate generation system is physically separate from a dialysis controller unit and wherein said dialysate generation system comprises a
25 container configured to hold fluid, wherein the container comprises an internal base surface and an outlet tube that is in fluid communication with a fluid pathway positioned in the dialysis controller unit and a base enclosure configured to detachably receive a bottom portion of the container, wherein said base enclosure comprises: a scale in physical communication with the bottom portion of the container and configured to weigh the fluid positioned within the container
30 and a conductivity sensor positioned proximate the bottom portion of the container and configured to measure a conductivity of the fluid in the container, the method comprising: filling

a predefined quantity of water into the container; placing the container in the base enclosure; adding at least one powdered composition to the water in the container to create dialysate fluid; weighing the dialysate fluid in the container using said scale; measuring a conductivity of the dialysate fluid in the container using said conductivity sensor; determining if the weight and
5 conductivity of the fluid in the container falls within a range of acceptable values for weight and conductivity; causing the dialysate fluid to flow from the outlet tube to the fluid pathway positioned in the dialysis controller unit; heating the dialysate fluid in the fluid pathway using an in-line heating element; and passing the dialysate fluid over a sorbent for filtration.

Optionally, the in-line heating element is a resistive heating element positioned
10 longitudinally along and cylindrically around said fluid pathway.

Optionally, the in-line heating element is an inductive heating element positioned longitudinally along and cylindrically around said fluid pathway.

Optionally, the container comprises an internal base surface that, relative to a substantially horizontal surface, has a slope in a range of 0.1 degrees to 50 degrees.

15 Optionally, the method further comprises adjusting a measured weight of the dialysate fluid to account for an unequal distribution of dialysate fluid across the internal base surface due to said slope in a range of 0.1 degrees to 50 degrees.

In some implementations, the present specification discloses a dialysate generation system for generating a dialysate fluid during a dialysis treatment, comprising: a dialysis machine
20 comprising a fluid circuit; a container configured to receive fluid from the fluid circuit, the container comprising: an outlet fluidically connected to the fluid circuit, and a bottom portion having a sloped internal surface having a slope of 0.1 degrees to 50 degrees; and a base configured to detachably connect to the bottom portion, the base comprising: a scale configured to weigh the container and fluid from the fluid circuit, and a conductivity sensor positioned
25 proximate the bottom portion and configured to measure a conductivity of the fluid from the fluid circuit.

The aforementioned and other implementations of the present specification shall be described in greater depth in the drawings and detailed description provided below.

30 **BRIEF DESCRIPTION OF THE DRAWINGS**

These and other features and advantages of the present invention will be further appreciated, as they become better understood by reference to the detailed description when considered in connection with the accompanying drawings:

FIG. 1 is a front view of an exemplary dialysis system;

5 FIG. 2 is a perspective view of the exemplary dialysis system of FIG. 1;

FIG. 3A illustrates an exemplary block diagram of a dialysate management system, in accordance with an implementation of the present specification;

10 FIG. 3B illustrates an exemplary block diagram of a dialysate container with one tube functioning as both an inlet and outlet, in accordance with an implementation of the present specification;

FIG. 3C illustrates an exemplary block diagram of a dialysate container with separate inlet and outlet tubes, in accordance with an implementation of the present specification;

15 FIG. 3D illustrates an exemplary block diagram of a dialysate container with one tube functioning as both an inlet and outlet and a sloped internal bottom surface, in accordance with an implementation of the present specification;

FIG. 3E illustrates an exemplary block diagram of a dialysate container with separate inlet and outlet tubes and a sloped internal bottom surface, in accordance with an implementation of the present specification;

20 FIG. 4A is a flowchart illustrating exemplary steps of using a dialysate management system in accordance with one implementation of the present specification;

FIG. 4B is a flowchart illustrating exemplary steps of using a dialysate management system in accordance with another implementation of the present specification; and

FIG. 5 illustrates an in-line heating element, in accordance with an implementation of the present specification.

25

DETAILED DESCRIPTION

While the present specification discloses inventions that are embodied in many different forms, for the purpose of promoting an understanding of the principles of the specification, reference will now be made to the embodiments illustrated in the drawings and specific language will be used to describe the same. Any alterations and further modifications in the described
30 embodiments, and any further applications of the principles of the specification as described

herein are contemplated and incorporated herein, as would normally occur to one skilled in the art to which the specification relates.

The term “and/or” means one or all of the listed elements or a combination of any two or more of the listed elements.

5 The terms “comprises” and variations thereof do not have a limiting meaning where these terms appear in the description and claims.

Unless otherwise specified, “a”, “an”, “the”, “one or more”, and “at least one” are used interchangeably and mean one or more than one.

10 For any method disclosed herein that includes discrete steps, the steps may be conducted in any feasible order. And, as appropriate, any combination of two or more steps may be conducted simultaneously.

Also herein, the recitations of numerical ranges by endpoints include all numbers subsumed within that range (e.g., 1 to 5 includes 1, 1.5, 2, 2.75, 3, 3.80, 4, 5, etc.). Unless otherwise indicated, all numbers expressing quantities of components, molecular weights, and so forth used in the specification and claims are to be understood as being modified in all instances by the term “about.” Accordingly, unless otherwise indicated to the contrary, the numerical parameters set forth in the specification and claims are approximations that may vary depending upon the desired properties sought to be obtained by the present specification. At the very least, and not as an attempt to limit the doctrine of equivalents to the scope of the claims, each numerical parameter should at least be construed in light of the number of reported significant digits and by applying ordinary rounding techniques.

20 Notwithstanding that the numerical ranges and parameters setting forth the broad scope of the specification are approximations, the numerical values set forth in the specific examples are reported as precisely as possible. All numerical values, however, inherently contain a range necessarily resulting from the standard deviation found in their respective testing measurements.

The present specification is directed towards multiple implementations. The following disclosure is provided to enable a person having ordinary skill in the art to practice the invention. Language used in this specification should not be interpreted as a general disavowal of any one specific implementation or used to limit the claims beyond the meaning of the terms used therein.

30 The general principles defined herein may be applied to other implementations and applications without departing from the spirit and scope of the invention. Also, the terminology and

phraseology used is for the purpose of describing exemplary implementations and should not be considered limiting. Thus, the present invention is to be accorded the widest scope encompassing numerous alternatives, modifications and equivalents consistent with the principles and features disclosed. For purpose of clarity, details relating to technical material that is known in the technical fields related to the invention have not been described in detail so as not to unnecessarily obscure the present invention.

It should be noted herein that any feature or component described in association with a specific implementation may be used and combined with any other implementation unless clearly indicated otherwise.

In an implementation, the present specification provides a dialysate management system or dialysate generation system that includes a dialysate container with a base enclosure, detached and separate from the dialysis system, which is configured to weigh any solution placed in the container, measure the conductivity of the solution in the container and, optionally, heat the solution or direct the solution through an in-line heating element. In one implementation, the dialysate management system is used in conjunction with a dialysis system and is connected via a wireless or wired interface to the controller, base unit and/or pump unit of the dialysis system. It should be noted herein that the terms dialysate management system and dialysate generation system may be used interchangeably.

In implementations, a pre-defined quantity of water is filled in the dialysate container and a pre-defined amount of prescription powder is mixed therein. In an implementation, a disposable liner or a disposable flexible container is fitted within the container for holding the prescription powder which eventually dissolves in the water filled in the container.

The present specification provides a dialysate management system which can rapidly heat dialysate without having to first transfer the dialysate to a reservoir bag which is typically heated within a dialysis machine. The dialysate management system includes a container configured to be placed on a portable base, holder, cozy, or other partial enclosure having a means to determine the conductivity and/or weight of the solution contained in the container, thereby eliminating the need for a dialysis machine used in conjunction with the container to comprise integrated heating and conductivity measurement elements and effectively reducing the weight of the dialysis machine. The dialysate container of the present specification reduces the number of steps and the time required in preparing a dialysis system for performing dialysis.

FIGS. 1 and 2 illustrate front and perspective views respectively, of a dialysis system 100, 200 with which the dialysate management systems of the present specification may be used. It should be apparent to those of skill in the art that the dialysis system 100, 200 shown in FIGS. 1 and 2 is merely exemplary and that the dialysate management system of the present specification
5 may be used with any type of dialysis system comprising a sorbent system, with or without an integrated reservoir system.

Referring to FIGS. 1 and 2 concurrently, the dialysis system 100, 200 comprises a top unit 101, 201 that is optionally connected to a bottom unit or base unit 102, 202. The bottom unit 102, 202 comprises a reservoir 122, 222 for fluid storage, measurement, and monitoring. The top
10 unit 101, 201, also referred to as the main unit or controller unit, comprises a graphical user interface 114, 214, a plurality of pumps, a processing unit for controlling the operating of the plurality of pumps, electronics, and a door 110, 210 with a power lock and mechanical backup mechanism.

In implementations, the top unit also provides electronic interfaces, such as Ethernet
15 connections or USB ports, to enable a direct connection to a network, thereby facilitating remote prescription verification, compliance vigilance, and other remote servicing operations. In addition, the electronic interfaces are used to transmit, either wired or wirelessly, the measured values of weight, conductivity, and temperature to the dialysis machine, which verifies the values and sends the confirmation back to the dialysate management system, as described in greater
20 detail below. The interfaces are electronically isolated, thereby ensuring patient safety regardless of the quality of the interfacing device.

In implementations, the graphical user interface 114, 214 provides for a simple user interface with the dialysis system 100, and includes maximal use of colors and a touch screen. The touch screen allows multiple user input configurations, provides multiple language
25 capability, and can be readily seen at night (particularly with brightness controls and night-vision colors).

The top unit 101, 201 further comprises handles 211 and a workspace in the form of a useable shelf 112, 212, also located at the top. The handles 211, located on the upper pumping portion of the system, are directly connected to the internal structure or frame of the system and
30 are not simply an extension of the exterior plastic molding, housing, or skins surrounding the top unit 101, 201. The direct connection to the internal frame of the system permits using the handle

to reposition the system in a manner that is safe and can reliably handle the load, particularly when the instrument is in operation with six liters of water (adding approximately 40 lbs). The bottom unit 102, 202 has a door 118 which, when opened or pulled out and not blocked by any protrusion, slides the reservoir 122 out, or otherwise makes the reservoir 122 accessible to a user,
5 to allow a user to insert or change fluids used for dialysis.

A clasp 105 is used to detachably affix a dialyzer 103 to a first side of the top unit 101, 201. A sorbent cartridge locking base 104, 204 used to detachably affix a sorbent cartridge 107 to a second, opposing side of the top unit 101, 201. It should be appreciated that in other implementations, the clasp, hemofilter, sorbent cartridge locking base, and sorbent cartridge can
10 be positioned on the same side of the top unit. In either case, the bottom unit 102, 202 has a sufficiently larger area relative to the top unit 101, 201 such that shelves are formed on either side of the top unit 101, 201 to hold the sorbent cartridge, to hold an infusate jar, to capture any spillage, and/or to channel any leaks into a leak detector.

Optionally, in an implementation, as shown in FIG. 1, between the dialyzer 103 and door
15 110 are anti-coagulant pumps in the form of syringe pumps 190. The use of the anti-coagulant syringe pump is optional. Optionally, the top unit 101, 201 can comprise a bottle holder that has a spiked base to receive a bottle, top-down, within the bottle holder housing. Infusion lines are connected to the inlet of the blood pump, outlet of the blood pump, or outlet of the dialyzer (blood side). The infusion lines could also 'thread' through air bubble detectors to sense if/when
20 the anti-coagulant is emptied or blocked.

In an implementation, the reservoir 122, 222 may be eliminated in favor of a dialysate management system that is remotely positioned relative to, and not physically attached to, the top unit 101, 201. In this case, the dialysate management system is separate from, and is not
25 physically connected to, the dialysis machine, but rather fluidically connected, thereby allowing it to be in a separate physical location from the dialysis machine, such as on the floor.

In conventional dialysis systems, the dialysate is pumped out from a container, such as a jug, and, after being subject to a priming process, is transferred into the reservoir 122, 222. The dialysate management system described in the present specification eliminates the need for a discrete reservoir integrated into the dialysis system, thereby enabling greater portability of the
30 dialysis system.

In implementations, the top unit 101, 201 of the dialysis system 100, 200 comprises a blood fluid path or circuit and a dialysate fluid paths or circuit, wherein the dialysate fluid circuit and blood fluid circuit are in fluid communication with the dialyzer and wherein the sorbent cartridge is in fluid communication with the dialysate fluid circuit. The patient's toxin-
5 containing blood is pumped from a blood vessel of the patient and is circulated, using a blood pump, in the blood circuit on one side of the membrane (dialyzer/dialyzer cartridge) and the dialysate, comprising the main electrolytes of the blood in concentrations prescribed by a physician, is circulated on the other side in the dialysate circuit. The circulation of dialysate fluid thus provides for the regulation and adjustment of the electrolytic concentration in blood.

10 The dialyzer cartridge used may be of any type suitable for hemodialysis, hemodiafiltration, hemofiltration, or hemoconcentration, as are known in the art. Used dialysate fluid from the dialyzer enters the dialysate circuit. In an implementation, a dialysate pump draws spent dialysate from the dialyzer cartridge and forces the dialysate into a dialysate regeneration system and back into the dialyzer cartridge in a multiple pass loop, thus generating “re-
15 generated” or fresh dialysate. Thus, a sorbent cartridge is provided in the dialysate circuit, which enables regeneration of fresh dialysate from the spent dialysate coming from the dialyzer. By regenerating the dialysate with sorbent cartridges, the dialysis system requires only a small fraction of the amount of dialysate of a conventional single-pass hemodialysis device.

A heater is also provided to maintain the temperature of dialysate fluid in the container at
20 the required level. The temperature of the dialysate fluid can be sensed by a temperature sensor located just before the fluid's entry into the dialyzer.

FIG. 3A illustrates an exemplary block diagram of a dialysate management system in accordance with an embodiment of the present specification. Each component in the dialysate management system 300 may be fabricated from any medical grade resilient material such as
25 stainless steel, polyethylene, polypropylene, polystyrene, PLA or other polymers. The dialysate management system comprises a container 324 and a base into which the container 324 is detachably positioned.

In an implementation, the container 324 is fabricated from molded plastic and is rectangular. In other implementations, the container 324 may be designed to have any suitable
30 shape, including polygonal and cylindrical. In an implementation, the container 324 also comprises a handle and a spout. In various implementations, the dimensions of the container 324

are in a range of approximately 10 to 14 inches high x 7.25 to 11.25 inches wide x 5.63 to 9.63 inches deep and the weight of the container 324 is in a range of approximately 15 to 25 pounds. In a preferred embodiment, the dimensions of the container 324 are 12 inches high x 9.25 inches wide x 7.63 inches deep and the container 324 weighs less than 20 pounds, thereby being easier
5 to lift and enabling the portability of the dialysis system. In various implementations, the container 324 has a capacity of approximately 2 to 4 gallons, or approximately 7.5 to 15 L. More specifically, when the dialysis system initiates operation, the container 324 holds at least 6 L of water. After treatment, the container 324 may hold up to 10 L of fluid, some of which has been removed from the patient. Therefore, the capacity of the container 324 is preferably in a
10 range of 12 L to 15 L.

In an implementation, the base 302 is positioned below and configured to receive a bottom surface 304 of the container 324. The base 302 is designed as a cozy, partial enclosure, container, or receiver configured to receive the container 324. The base 302 includes a top surface 340 for receiving at least a portion of the bottom surface 304 of container 324.
15 Preferably, the walls of the container 324 are flexible to facilitate placement into and removal from the base 302. The container 324 conforms to the shape of the base 302 for proper fit, in one implementation, but does not lose its shape. In an embodiment, the top surface 334 of the base 302 is substantially horizontal, or parallel to the bottom external surface 344 of the base 302. In various implementations, the dimensions of the base 302 are in a range of approximately 12 to
20 16 inches wide x 8 to 10 inches deep x 3 to 7 inches high, preferably the dimensions of the base enclosure are 14 inches wide x 10 inches deep x 5 inches high.

The dimensions of the container 324 are preferably designed to be as small as possible, thereby improving portability, while still allowing for a container volume sufficient to contain all the requisite dialysate. Similarly, the base 302 is preferably designed to be as small while still
25 being capable of receiving the bottom surface of the container 324.

In some implementations, the bottom surface 304 of the container 324 is substantially horizontal, or parallel to the bottom external surface 344 of the base 302, and not sloped or tilted. In some implementations, however, the bottom surface 304 of the container 324 is sloped or tilted to ensure complete removal of fluid from the container. Referring to FIGS. 3B and 3C, an
30 outlet tube 322, 334 is placed proximate to the base of the container to ensure complete removal of fluid from the container, as further described below. The outlet tube 322, 334 is in fluid

communication with the dialysis system via a tubing that connects the outlet tube 322, 334 to a disposable manifold housed within the dialysis system for filtration.

In one implementation, the height from the bottom of the container 324 where the outlet tube(s) or port(s) is placed ranges from $\frac{1}{4}$ to $\frac{1}{2}$ inch. One of ordinary skill in the art would appreciate that if the outlet tube or port is placed too high from the bottom of the container 324, it will lead to a fluid residue in the container 324, even if the base of the container 324 is tilted. In an implementation, fluid is drawn from the container 324 by the pump action of the pumping unit of the dialysis system.

FIGS. 3B and 3C illustrate block diagrams of dialysate containers having straight (non-tilted) internal and external bottom surfaces, in accordance with some implementations of the present specification. Referring to FIG. 3B, there is one tube 322 in fluid communication with the internal volume of the container 324, which can function as an inlet or outlet, depending on the stage of treatment. In another implementation, referring to FIG. 3C, there are two tubes 332, 334 in fluid communication with the internal volume of the container 324, with a first tube 332 acting as an inlet and a second tube 334 acting as an outlet. In this case, fluid is returned to the container 324 after treatment and is re-circulated through the system.

In an implementation, the bottom 351 of the container 324 is internally sloped to allow for greater fluid removal. The angle of the slope or tilt of the internal bottom surface 351 of the container 324 ranges from 0.1 degrees to 50 degrees relative to a substantially horizontal surface. FIGS. 3D and 3E illustrate block diagrams of containers 324 having internally sloped bottom "floors" 351, in accordance with some implementations of the present specification. Referring to FIG. 3D, one tube 352 is in fluid communication with the internal volume of the container 324 and extends out from the container 324 to thereby function as an inlet or outlet, depending on the stage of treatment. In another implementation, referring to FIG. 3E, there are two tubes 362, 364 in fluid communication with the internal volume of the container 324 and extending out from the container 360, with a first tube 362 configured as an inlet and a second tube 364 configured as an outlet. In this case, fluid may be returned to the container 324 after treatment and is re-circulated. As shown, the container 324 includes an internal sloped bottom floor 351 to direct fluid to the tubes 352, 364 respectively. The external bottom surface of the container may or may not reflect the tilt, or slope, of the internally sloped surface 351.

In one implementation, the height from the bottom of the container 324 where the outlet tube(s) or port(s) is placed ranges from $\frac{1}{4}$ to $\frac{1}{2}$ inch. In an embodiment, a placement at $\frac{1}{4}$ inch or lower may represent the lowest point at which the outlet tube is positioned proximate to a sloped internal base surface and opposite from the highest point of said sloped internal base surface, wherein the highest point may be represented by a placement of $\frac{1}{4}$ to $\frac{1}{2}$ inch proximate to said sloped internal base surface. One of ordinary skill in the art would appreciate that if the outlet tube or port is placed too high from the bottom of the container 324, it will lead to a fluid residue in the container 324, even if the base of the container 324 is tilted. In an implementation, fluid is drawn from the container 324 by the pump action of the pumping unit of the dialysis system.

Referring back to FIG. 3A, the base 302 comprises a weighing mechanism 308, such as a scale, for measuring the weight of the container 324 when water and/or compositions are placed into the container 324. The base 302 further optionally includes a battery 310 for power and a wireless transmitter 312 for wirelessly connecting to the dialysis machine for conveying the weight, conductivity and/or temperature of the dialysate solution to the dialysis machine without requiring a physical data connection to the dialysis machine. In another, less preferred implementation, the base 302 may be remote from, yet wired to, the dialysis machine to receive power and to transmit data.

In a preferred implementation, the container 324 is in fluid communication with an in-line heating mechanism, thereby enabling fluid to be heated as it flows through a pipe and without statically storing fluid for heating. Thus, the required dialysate may be heated to a desired temperature as it circulates through the dialysis system, without first having to wait for the dialysate to be heated in a reservoir. Referring to FIG. 5, in an implementation, the in-line heating mechanism 554 is a resistive or inductive heating element that is positioned longitudinally along, and in temperature communication with, a fluid pathway 584 extending from the container 324 to and/or through a manifold positioned within the dialysis system 100. The resistive heating element may comprise a plurality of wires that are in electrical communication with a controller configured to adjustably deliver electricity to the wires and, to generate heat when current is applied thereto, thereby increasing the temperature of proximate structures (e.g., including the fluid pathway 584). The inductive heating element may comprise a ferromagnetic material positioned on or cylindrically around the fluid pathway and an inductor sleeve cylindrically positioned around the ferromagnetic material. The inductor sleeve is in

electrical communication with a controller configured to adjustably deliver electricity to the sleeve such that, when current is applied thereto, a magnetic field is created in the sleeve causing the nearby ferromagnetic material to heat up, thereby increasing the temperature of proximate structures (e.g., the fluid pathway 584) as well. Preferably, the heating element 554 is located in
5 a pump unit relatively close to the blood filter of the dialysis system so that a minimum of heat energy is lost as the fluid moves through the heating element 554 to the required portions of the dialysis circuit.

In an alternative implementation, the base 302 may comprise an integrated heating element 376, for heating fluid in the container 324 to a predefined temperature. The heating
10 element 376 may be an inductive heating element having a ferromagnetic base in physical communication with the container 324 and an inductor circuit positioned below the ferromagnetic base. The inductor circuit is in electrical communication with a controller in the base 302 configured to adjustably deliver electricity to the circuit such that, when current is applied thereto, a magnetic field is created in the circuit causing the nearby ferromagnetic base to
15 heat up, thereby causing proximate structures, including the base of the container 324, to increase in temperature as well. The dialysate placed in the container 324 may, therefore, be pre-heated and primed to a desired temperature by using the base 302.

Referring back to FIG. 3A, in an implementation, a disposable sealable liner 306 is fitted within the container 324 of dialysate management system 300 above the bottom surface 304 of
20 the container, as shown. The liner 306 may be made of a porous material and is designed to hold powdered compositions within a sealed compartment. When water is poured into the container 324, the water enters the porous liner 306 and the prescription is dissolved into the water producing the required dialysis solution. The liner 306 may include a fitting 307, positioned at the top of the liner, to which a prescription bag 309 containing the powdered compositions is
25 attached such that, when water is poured into the container 324, the powdered compositions dissolve in the water producing the required dialysate. In an implementation, the fitting comprises a screw fitting. In another implementation, wherein the container does not include a liner, a fitting for affixing a prescription bag is included on the container itself. In another implementation, a prescription “pod” containing the powdered compositions in a porous
30 substrate may be dropped into the container 324, which already is filled with a predefined quantity of water. The prescription pod then dissolves in the water producing the required

dialysate. In another implementation, a second disposable, porous flexible container is fitted within the container 324 and configured to contain the powdered compositions, which eventually dissolve in the water that fills the container 324.

Where the container 324 includes a spout, a disposable liner may be folded and directed
5 into the spout such that it fills the appropriate space. In one implementation, the liner adapts to the threads of the opening of the container, which is capped using a cap assembly. A fitting, such as a luer fitting with $\frac{1}{4}$ turn, is provided on the top of the cap. In one implementation, the liner is attached to another plastic component that holds a fitting. In an implementation, a portion of the
10 liner is folded over the mouth of the container opening, and a plastic component is screwed onto a thread on the mouth of the opening, which fixes the liner in place. This arrangement is similar to a bottle cap or a bottle adapter, which is mated to the bottle by a screw mechanism.

It may be noted that since the liner is porous, it acts as a mesh or net and does not block or stop the flow of fluid to the outlet tube from the container. The liner is separate from the port opening, pick-up tube, or inlet/outlet tube at the bottom of the container. In some embodiments,
15 the liner comprises notches such that a portion of the liner is sucked into an outlet tube and conforms to the shape of the tube, without blocking flow through the outlet tube. In some embodiments, the liner is configured as a plastic cage or net and acts as a porous ball on the outlet tube (a circular portion of the liner is pulled into the outlet tube) without blocking flow through the outlet tube.

20 In an implementation, the base 302 comprises a single, centrally located flexure assembly (not shown) for measuring the weight of the container 324 by using load cells and/or strain gauges. The flexure assembly may be mounted to the underside surface of the base 302 and include mounting plates, magnets, flexure rings, spacers, and a circuit board.

In another implementation, weight measurement is achieved using hall sensors and a
25 circuit board integrated into the base 302. Hall sensors on the circuit board resistively sense changes in magnetic fields generated by the movement of the magnets for calculation of weight measurements. The circuit board and hall sensors are stationary and two sets of magnets, one above the board and another below the board, move vertically in relation to the board and fixed in relation to each other. The hall sensors sense the change in the magnetic field as the sets of
30 magnets move when weight is applied to the base 302. The change in the magnetic field causes an output in voltage from the hall sensors. A processor on the circuit board processes the voltage

output to determine the weight. Use of a flexure assembly with one axis of movement provides a scale system that is low cost, reliable, robust and easy to assemble and integrate into the base 302, as described in United States Patent Number 9,157,786, which is incorporated herein by reference in its entirety. In implementations where the bottom of the container is sloped or tilted,
5 the measured weight is mathematically adjusted using the angle of the tilt to compensate for weight not being measured on a level platform.

The base 302 preferably further comprises a conductivity measurement system 316 to measure the conductivity of the solution contained within the container 324. A conductivity coil, configured to generate a field and use changes in that field to measure conductivity, may be
10 integrated into base 302 and positioned proximate the bottom surface of the container. Accordingly, when the container 324 is placed on base 302, it is heated and, because it is in contact with the conductivity coil, its conductivity is also monitored. In one implementation, the conductivity is measured using a conductivity coil, as described in United States Patent Number 9,201,036, which is incorporated herein by reference in its entirety.

15 In an implementation, a non-invasive detection method based on ultrasonic time of flight (TOF) measurement is used to measure the conductivity and/or density of the solution contained in the container 324. The base 302 is provided with one or more ultrasonic sensors for non-invasive measuring of the conductivity and/or density of the fluid. The ultrasonic sensors also measure the level of the fluid in the container, providing differential redundancy with the weight
20 measurement load cells to determine the amount of fluid in the container 324. The combination of load cells and ultrasonic sensors provides an accurate and reliable measurement of the weight and conductivity of the solution contained in the container 324. In embodiments, the accuracy of the load cells and/or ultrasonic sensors are within 5% of actual physical measurements of the conductivity, density, weight, and/or level of the fluid.

25 FIG. 4A is a flowchart illustrating exemplary steps of using a container 324 of the present specification. At step 402, the container 324 is filled with a predefined quantity of water and placed on a base 302. At step 404, a predefined amount of prescribed materials, in the form of powdered compositions, is added to the water in the container 324. The powdered compositions may be in a loose powder form, in the form of a prescription pod, or in the form of a disposable
30 lining positioned within the container 324, such that when water is poured into the container 324, the water enters the liner and the powdered compositions dissolve in the water producing the

required dialysate. In implementations, the predefined amount of prescribed materials or powdered compositions is dependent upon a physician's prescription for a particular user. Further the acceptable ranges of weight and conductivity are, in turn, dependent upon the nature of the user's prescription. In implementations, the controller unit is programmed in accordance
5 with the user's prescription. In implementations, an acceptable weight range range, in accordance with a user's prescription(s), is stored in an internal memory so that it can be compared to a measured weight. In implementations, an acceptable conductivity range, in accordance with a user's prescription(s), is stored in an internal memory so that it can be compared to a measured conductivity.

10 At step 406, the solution in the container 324 is weighed by one of the aforementioned weighing mechanisms integrated into the base 302. At step 408, the conductivity of the solution in the container 324 is measured using a conductivity coil provided within the base enclosure. At step 410, the solution in the container 324 is heated. In one implementation, the solution is heated using an in-line heating mechanism external to the base 302. This allows water or fluid to
15 be heated as it flows through a fluid pathway, and does not require the fluid to be statically stored for heating. Thus, water is heated to a desired temperature as it circulates through the dialysis system. In another implementation, the solution in the container 324 may be heated by a heating element provided within the base 302.

At step 412, data regarding the weight, conductivity and/or temperature of the dialysate is
20 transmitted from the base 302 to the controller positioned in the top unit 101 of dialysis system 100. Where an in-line heater is used external to the base 302, a temperature sensor positioned after the in-line heater is configured to measure the fluid temperature and transmit the requisite temperature data to the controller. The controller in the top unit 101 of dialysis system 100 determines if one or more of the weight, conductivity, and temperature of the solution in the
25 container 324 is equal to, or falls within, a predefined weight, temperature, and conductivity range. If the weight, conductivity, and/or temperature do not equal or fall within predefined value ranges, an alarm is triggered requiring the container 324 to be weighed again (and water may be added or removed from the container), conductivity to be measured again, and heating to be repeated or continued until the desired values are met. If the weight, conductivity, and
30 temperature equal or fall within predefined value ranges, at step 414, the dialysate solution is passed through a sorbent cartridge for filtration.

FIG. 4B is a flowchart illustrating exemplary steps of using the dialysate management system in accordance with another implementation of the present specification. At step 422, the container 324 is filled with a predefined quantity of water and placed on base 302. At step 424, a predefined amount of a prescribed powdered compositions is added to the water in the container 324. The powdered compositions may be in a loose powder form, the form of a prescription pod, or in the form of a disposable lining positioned within the container 324, such that when water is poured into the container 324, the water enters the liner, and the powdered compositions dissolve in the water producing the required dialysate. At step 426, the solution in the container 324 is weighed by one of the aforementioned weighing mechanisms provided within the base 302. At step 428, the base 302 transmits the weight data to the controller in the portable dialysis system and the controller compares the measured weight to a predetermined target weight and displays the comparison on a graphical user interface (GUI), where the GUI is located either on a visual display integrated into container 324 or base 302 or the portable dialysis system. The user then either adds more water or removes water if the measured weight is not equal to or proximate the predetermined target weight at step 432. If the measured weight is equal to or proximate the predetermined target weight, the user advances to the next step at step 430. In various implementations, a measured weight is considered sufficiently proximate if it falls within +/- 10% of the predetermined target weight. If the user adds more water at step 432, then the solution is weighed again at step 426, and the process iterates accordingly.

At step 434, the conductivity of the solution in the container 324 is measured as described above using a conductivity coil integrated into the base 302 and the conductivity data is transmitted to the controller in the dialysis system. At step 436, the controller compares the measured conductivity to a predetermined target conductivity for treatment and displays the comparison on a graphical user interface (GUI), where the GUI is located either on a visual display integrated into container 324 or base 302 or the portable dialysis system. The user then either adds more powdered compositions or water if the measured conductivity is not equal to or proximate the predetermined target conductivity at step 440 or advances to the next step if the measured conductivity is equal to or proximate the predetermined target conductivity at step 438. In various implementations, a measured conductivity is considered proximate if it falls within +/- 10% of the predetermined target conductivity. If the user adds more prescription or water at step

440, then the solution conductivity is measured again at step 434, and the process iterates accordingly.

At step 442, the solution in the container 324 is heated. In one implementation, the solution is heated using an external, in-line heating mechanism as described above. This allows
5 water or fluid to be heated as it flows through a pipe or a container, and does not require the fluid to be stored for heating. Thus, water is heated to a desired temperature as it circulates through the dialysis system. In an implementation, the heating element is located in the controller portion of top unit 101 of the dialysis system 100 relatively close to the blood filter so that a minimum amount of heat energy is lost as the fluid moves from the heating element to the filter. In an
10 alternate implementation, the solution in the container 324 may be heated by a heating element provided within the base 302.

At step 444, the temperature of the solution in the container 324 is measured by a temperature sensor. In an implementation, the temperature is measured by a temperature sensor installed in the base 302. In another implementation, the temperature of the solution may be
15 measured by a temperature sensor positioned external to the container 324 or the base 302. Data from the temperature sensor is transmitted to the controller of the dialysis unit. At step 446, the controller compares the measured temperature to a predetermined target temperature for treatment and displays the comparison on a graphical user interface (GUI), where the GUI is located either on a visual display integrated into container 324 or base 302 or the portable
20 dialysis system. The user then either allows the solution to continue to heat or cool if the measured temperature is not equal to or proximate the predetermined target temperature at step 450 or advances to the next step if the measured temperature is equal to or proximate the predetermined target temperature at step 448. In various implementations, a measured temperature is considered proximate if it falls within +/- 10% of the predetermined target
25 temperature. If the user allows the solution to continue to heat or cool at step 450, then the solution temperature is measured again at step 444, and the process iterates accordingly. At step 452, the solution is passed through a sorbent cartridge for filtration if the weight, conductivity, and temperature of the solution in the container are equal to or proximate a predefined weight, conductivity, and temperature as determined by the dialysis system.

30 In implementations, retrofitting any conventional dialysis system with the novel disclosed dialysate management system and removing or not using the conventional reservoir system will

result in a decrease of at least 10%, preferably upwards or 40% and any increment therein, of priming time associated with the generation of filtered, heated dialysate from a dialysate mixture.

In an implementation, the measured values of weight, conductivity, and temperature are wirelessly transmitted to the dialysis machine, which verifies the values and sends the
5 confirmation back to the base 302. In another implementation, the measured values are communicated using a wired connection between the container 324/base 302 and the dialysis system. In some implementations, the wired connection functions as a backup line if the wireless connection fails and comprises a USB, serial, or parallel connection. In yet another
10 implementation, the measured values are manually inputted to the dialysis system using a user interface. In some implementations, the interface is located on the container 324 and/or base 302. In other implementations, the interface is the same interface that is located on the dialysis system. In various implementations, the user interface, either on the container 324, the base 302 or top
15 unit 101 of the dialysis system 100, display indications to the user that the weight or conductivity of the container contents do not match predetermined values and to add more prescription or fluid, or the temperature of the fluid does not match a predetermined value, and that further heating is required. In some implementations, the indications include visual and audible
indications, including, but not limited to, digital displays, colored icons, and audio alarms.

In some implementations, the container 324 is equipped with indicator lights and/or a display panel, which indicates power and measured readings. In another implementation, the user
20 interface of the dialysis system (shown as 114 and 214 in FIG. 1 and FIG. 2) is used to display the measured readings and status values from the container 324 and base 302. In an implementation, power is supplied to the container 324 and base 302 using a rechargeable battery that can be charged by the main power unit of the dialysis system. In other
implementations, power is supplied to the container/enclosure via a USB cable or power cord.

25 The above examples are merely illustrative of the many applications of the reservoir bag of the present specification. Although only a few embodiments of the present specification have been described herein, it should be understood that the present specification might be embodied in many other specific forms without departing from the spirit or scope of the specification. Therefore, the present examples and embodiments are to be considered as illustrative and not
30 restrictive, and the specification may be modified within the scope of the appended claims.

CLAIMS**We claim:**

1. A dialysate generation system for generating a dialysate fluid during a dialysis treatment, comprising:
 - a container configured to hold fluid, wherein the container comprises an internal base surface that, relative to a substantially horizontal surface, has a slope in a range of 0.1 degrees to 50 degrees and an outlet tube that is in fluidic communication with a fluid circuit of a dialysis system; and
 - a base enclosure configured to detachably receive a bottom portion of the container, wherein said base enclosure comprises:
 - a first scale in physical communication with the bottom portion of the container and configured to weigh the fluid positioned within the container; and
 - a conductivity sensor positioned proximate the bottom portion of the container and configured to measure a conductivity of the fluid in the container.
2. The dialysate generation system of claim 1, wherein the container further comprises powdered compositions enclosed within a disposable porous material.
3. The dialysate generation system of claim 1, wherein the outlet tube is positioned proximate to a lowest point of said sloped internal base surface and opposite from the highest point of said sloped internal base surface.
4. The dialysate generation system of claim 3, wherein said outlet tube is positioned at a height ranging from $\frac{1}{4}$ to $\frac{1}{2}$ inch from an external bottom surface of said container.
5. The dialysate generation system of claim 1, further comprising a wireless transmitter configured to wirelessly transmit at least one of weight data and conductivity data to a controller in a dialysis machine, wherein said dialysis machine is in electronic communication with said dialysate generation system.

6. The dialysate generation system of claim 1, wherein the first scale comprises a flexure assembly.
7. The dialysate generation system of claim 6, wherein the flexure assembly comprises at least one of a load cell or strain gauge.
8. The dialysate generation system of claim 1, wherein the conductivity sensor comprises a conductivity coil.
9. The dialysate generation system of claim 1, wherein the conductivity sensor comprises ultrasonic sensors.
10. The dialysate generation system of claim 1, wherein the base enclosure and container are physically separate from the dialysis system and wherein the container and base lack a heating element.
11. A dialysis system, comprising:
 - a dialysis machine comprising:
 - a dialysate fluid circuit having a fluid pathway and a blood fluid circuit,
 - a dialyzer in fluid communication with the dialysate fluid circuit and blood fluid circuit,
 - a sorbent cartridge in fluid communication with said dialysate fluid circuit,
 - a plurality of pumps in physical communication with the dialysate fluid circuit and the blood fluid circuit,
 - a processing unit for controlling an operation of the plurality of pumps, and
 - a heating element configured to heat fluid as it flows through the fluid pathway;
 - and
 - a dialysate generation system physically separate from said controller unit, the dialysate generation system comprising:
 - a container configured to hold fluid, wherein the container comprises an outlet tube that is in fluid communication with said fluid pathway in the dialysate fluid circuit, a bottom portion, and an internal base surface, and

a base enclosure configured to detachably receive the bottom portion of the container, wherein said base enclosure comprises:

a scale in physical communication with the bottom portion of the container and configured to weigh the fluid positioned within the container; and

a conductivity sensor configured to measure a conductivity of the fluid in the container.

12. The dialysis system of claim 11, wherein the heating element is a resistive heating element positioned longitudinally along and cylindrically around said fluid pathway.
13. The dialysis system of claim 11, wherein the heating element is an inductive heating element positioned longitudinally along and cylindrically around said fluid pathway.
14. The dialysis system of claim 11, wherein the container comprises an internal base surface that, relative to a substantially horizontal surface, has a slope in a range of 0.1 degrees to 50 degrees.
15. The dialysate system of claim 14, wherein the outlet tube is positioned proximate to a lowest point of said sloped internal base surface and opposite from the highest point of said sloped internal base surface.
16. The dialysate system of claim 15, wherein said outlet tube is positioned at a height ranging from $\frac{1}{4}$ to $\frac{1}{2}$ inch from an external bottom surface of said container.
17. The dialysate system of claim 11, wherein the container further comprises powdered compositions enclosed within a disposable porous material.
18. The dialysate system of claim 11, further comprising a wireless transmitter configured to wirelessly transmit at least one of weight data and conductivity data to the processing unit.

19. A method of generating dialysate using a dialysate generation system, wherein said dialysate generation system is physically separate from a dialysis controller unit and wherein said dialysate generation system comprises a container configured to hold fluid, wherein the container comprises an internal base surface and an outlet tube that is in fluid communication with a fluid pathway positioned in the dialysis controller unit and a base enclosure configured to detachably receive a bottom portion of the container, wherein said base enclosure comprises:

a scale in physical communication with the bottom portion of the container and configured to weigh the fluid positioned within the container and

a conductivity sensor positioned proximate the bottom portion of the container and configured to measure a conductivity of the fluid in the container, the method comprising:

filling a predefined quantity of water into the container;

placing the container in the base enclosure;

adding at least one powdered composition to the water in the container to create dialysate fluid;

weighing the dialysate fluid in the container using said scale;

measuring a conductivity of the dialysate fluid in the container using said conductivity sensor;

determining if the weight and conductivity of the fluid in the container falls within a range of acceptable values for weight and conductivity;

causing the dialysate fluid to flow from the outlet tube to the fluid pathway positioned in the dialysis controller unit;

heating the dialysate fluid in the fluid pathway using an in-line heating element;
and

passing the dialysate fluid over a sorbent for filtration.

20. The method of claim 19, wherein the in-line heating element is a resistive heating element positioned longitudinally along and cylindrically around said fluid pathway.

21. The method of claim 19, wherein the in-line heating element is an inductive heating element positioned longitudinally along and cylindrically around said fluid pathway.

22. The method of claim 19, wherein the container comprises an internal base surface that, relative to a substantially horizontal surface, has a slope in a range of 0.1 degrees to 50 degrees.
23. The method of claim 22, further comprising adjusting a measured weight of the dialysate fluid to account for an unequal distribution of dialysate fluid across the internal base surface due to said slope in a range of 0.1 degrees to 50 degrees.
24. A dialysate generation system for generating a dialysate fluid during a dialysis treatment, comprising:
- a dialysis machine comprising a fluid circuit;
 - a container configured to receive fluid from the fluid circuit, the container comprising:
 - an outlet fluidically connected to the fluid circuit, and
 - a bottom portion having a sloped internal surface having a slope of 0.1 degrees to 50 degrees; and
 - a base configured to detachably connect to the bottom portion, the base comprising:
 - a scale configured to weigh the container and fluid from the fluid circuit, and
 - a conductivity sensor positioned proximate the bottom portion and configured to measure a conductivity of the fluid from the fluid circuit.

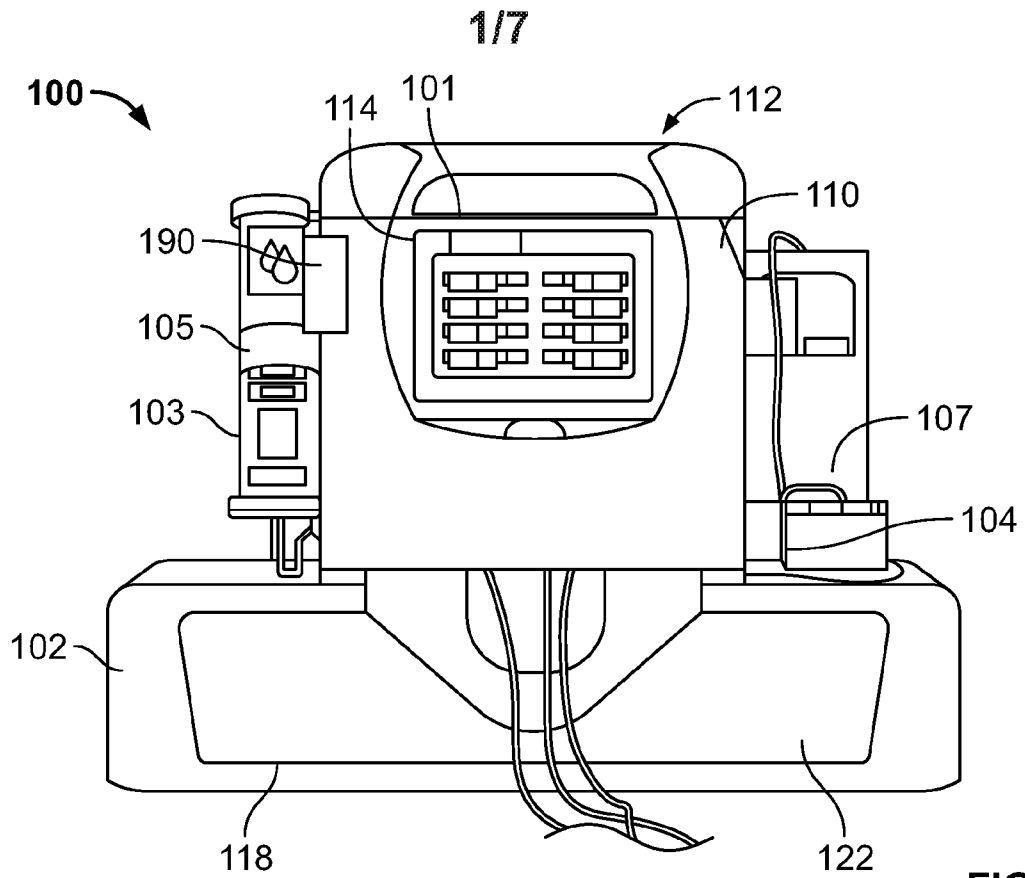


FIG. 1

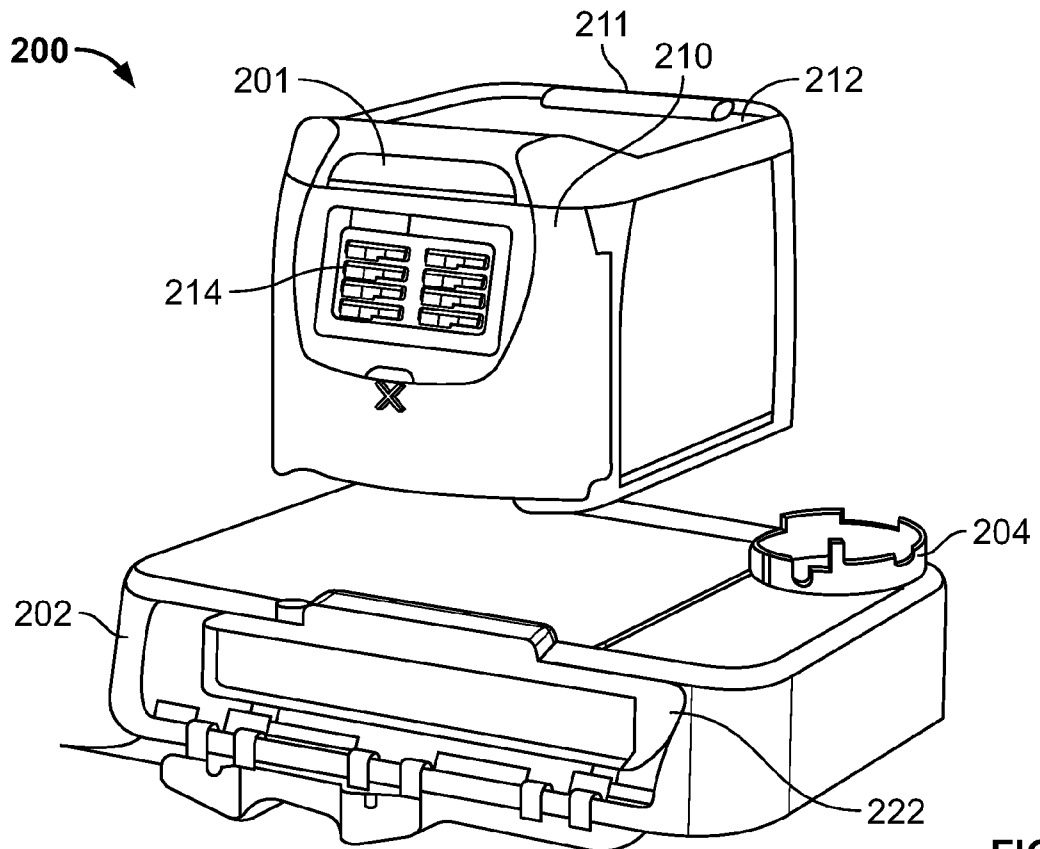


FIG. 2

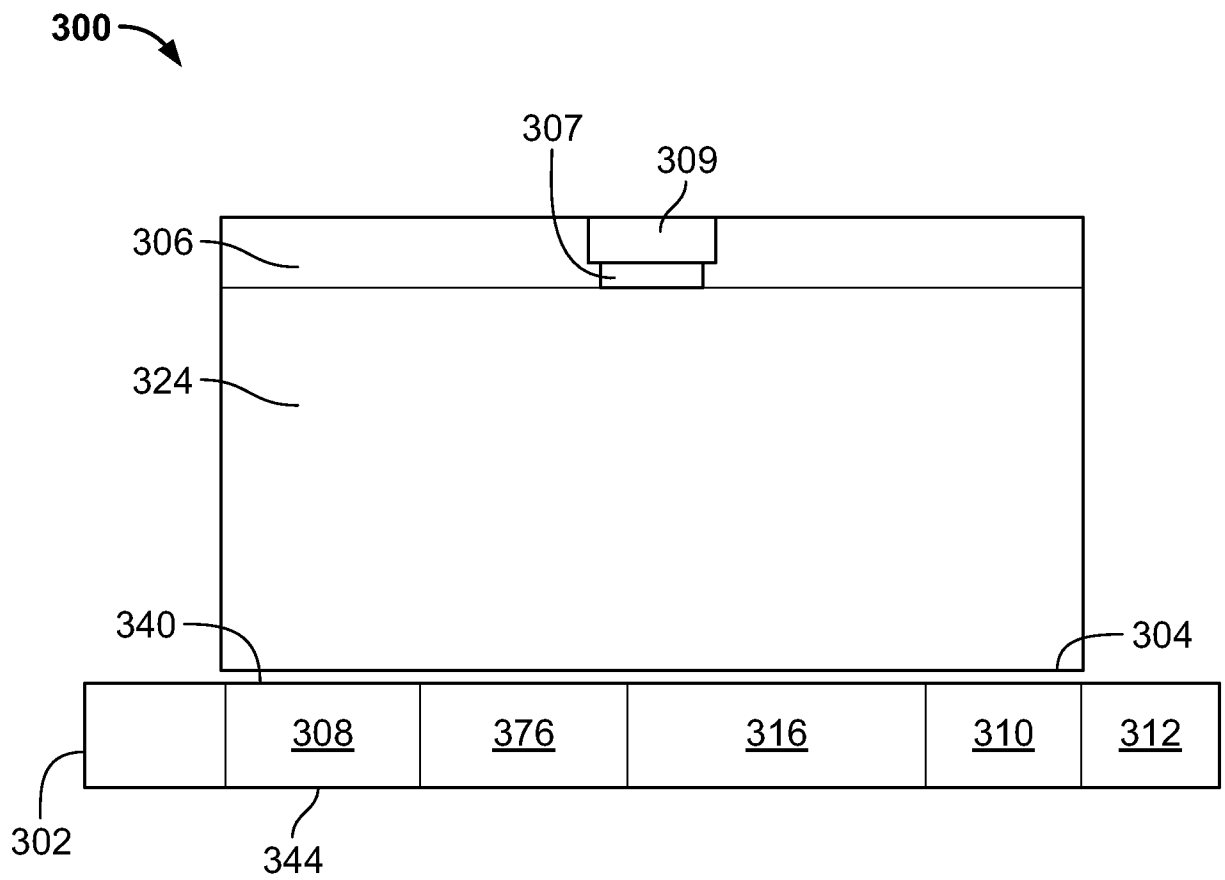


FIG. 3A

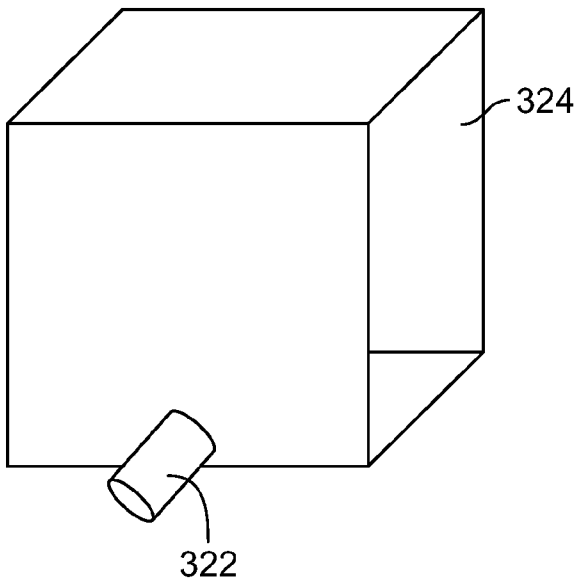


FIG. 3B

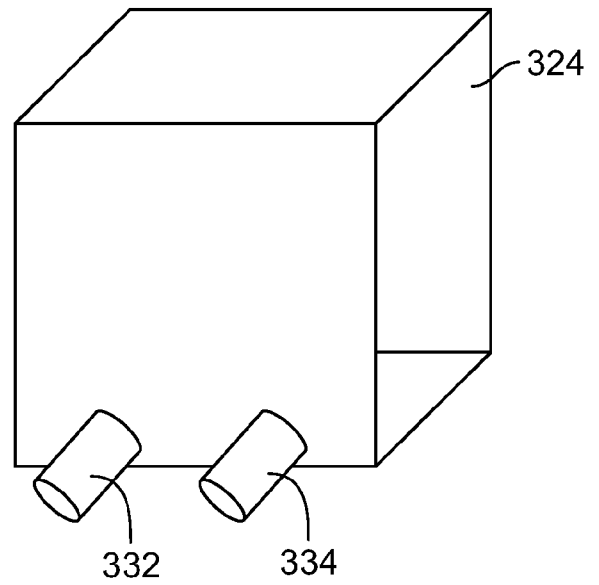


FIG. 3C

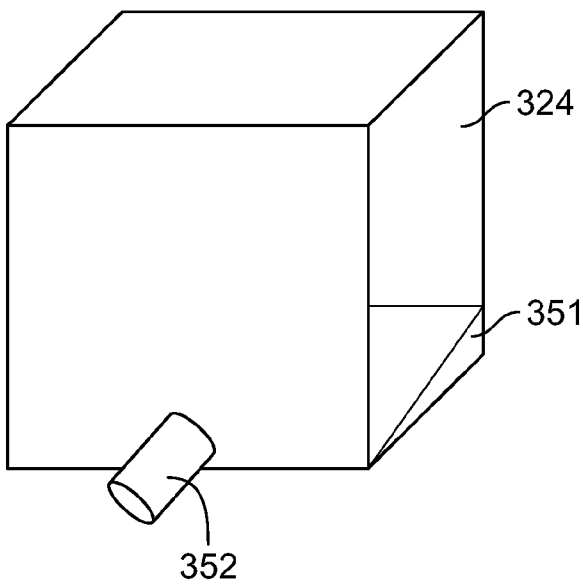


FIG. 3D

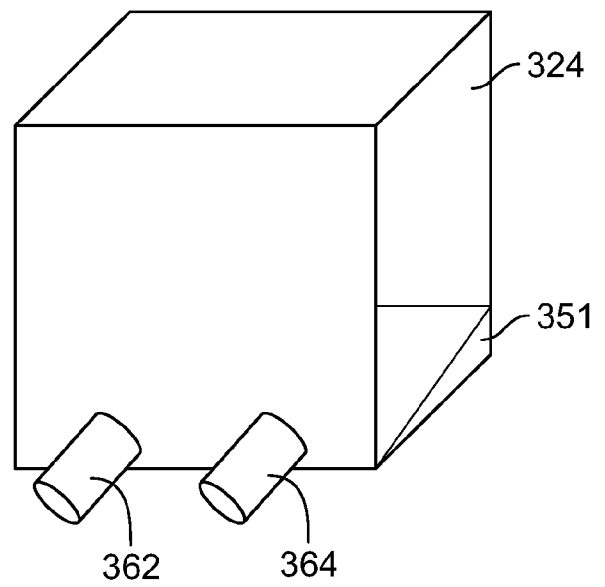


FIG. 3E

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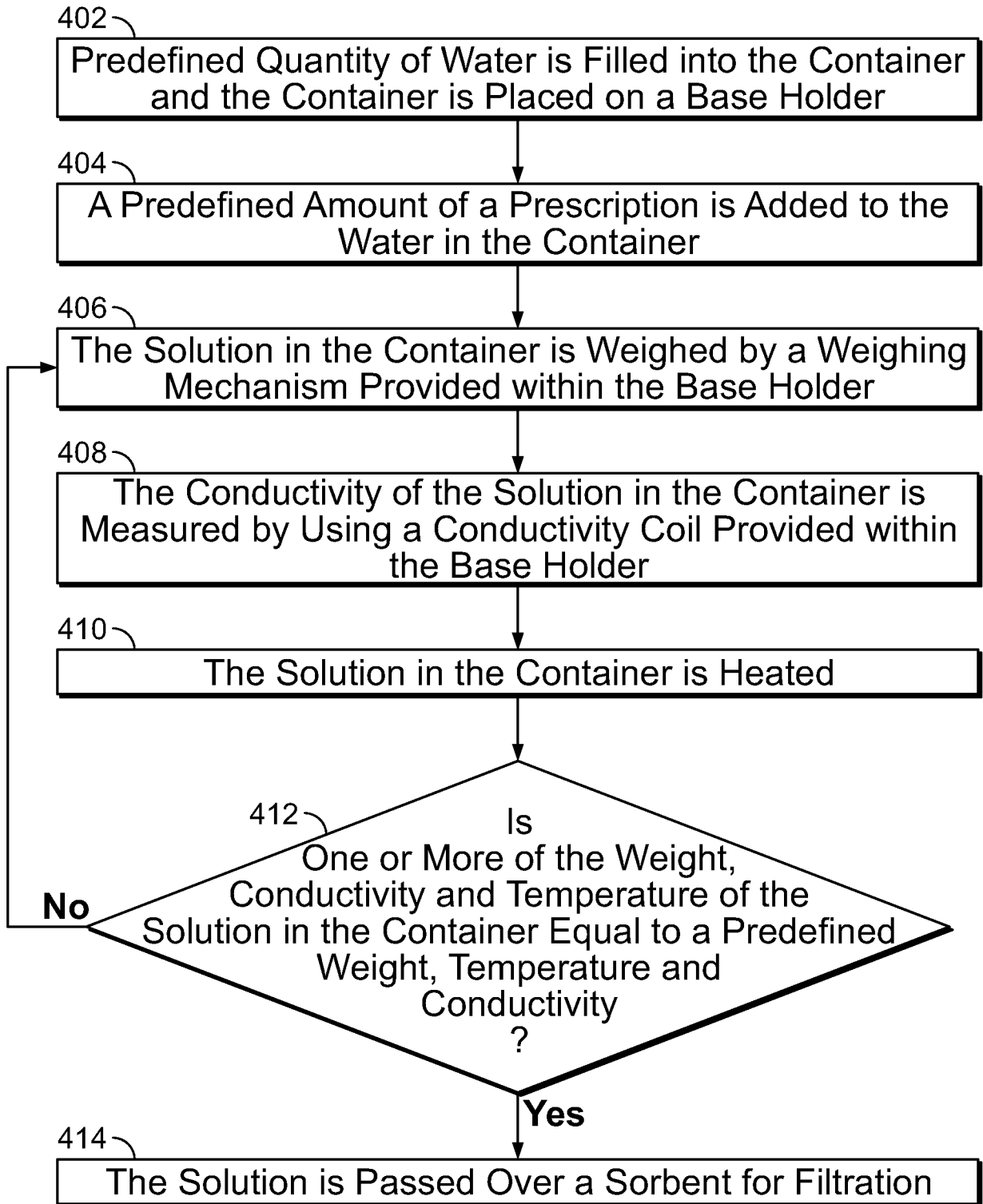


FIG. 4A

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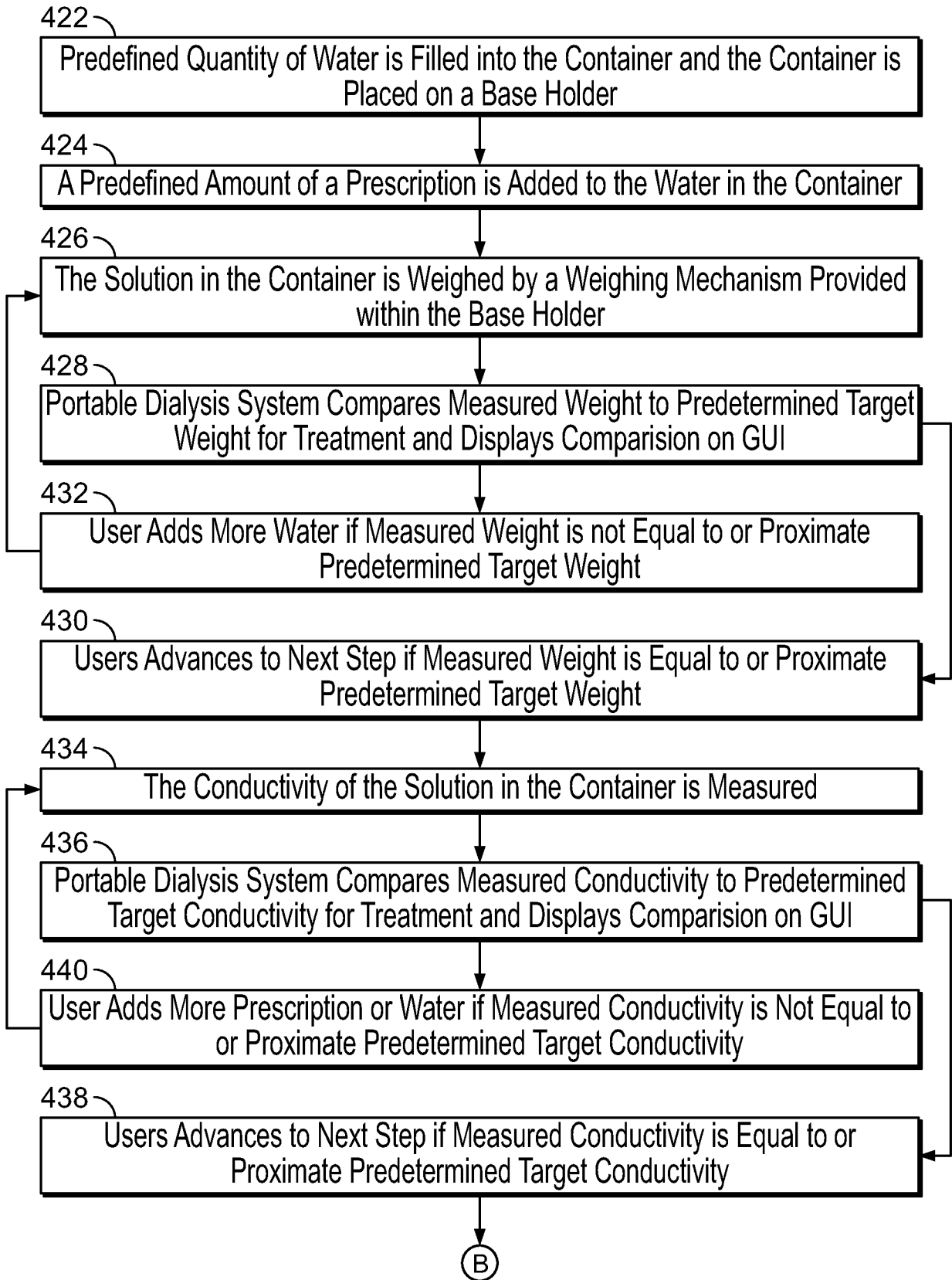


FIG. 4B

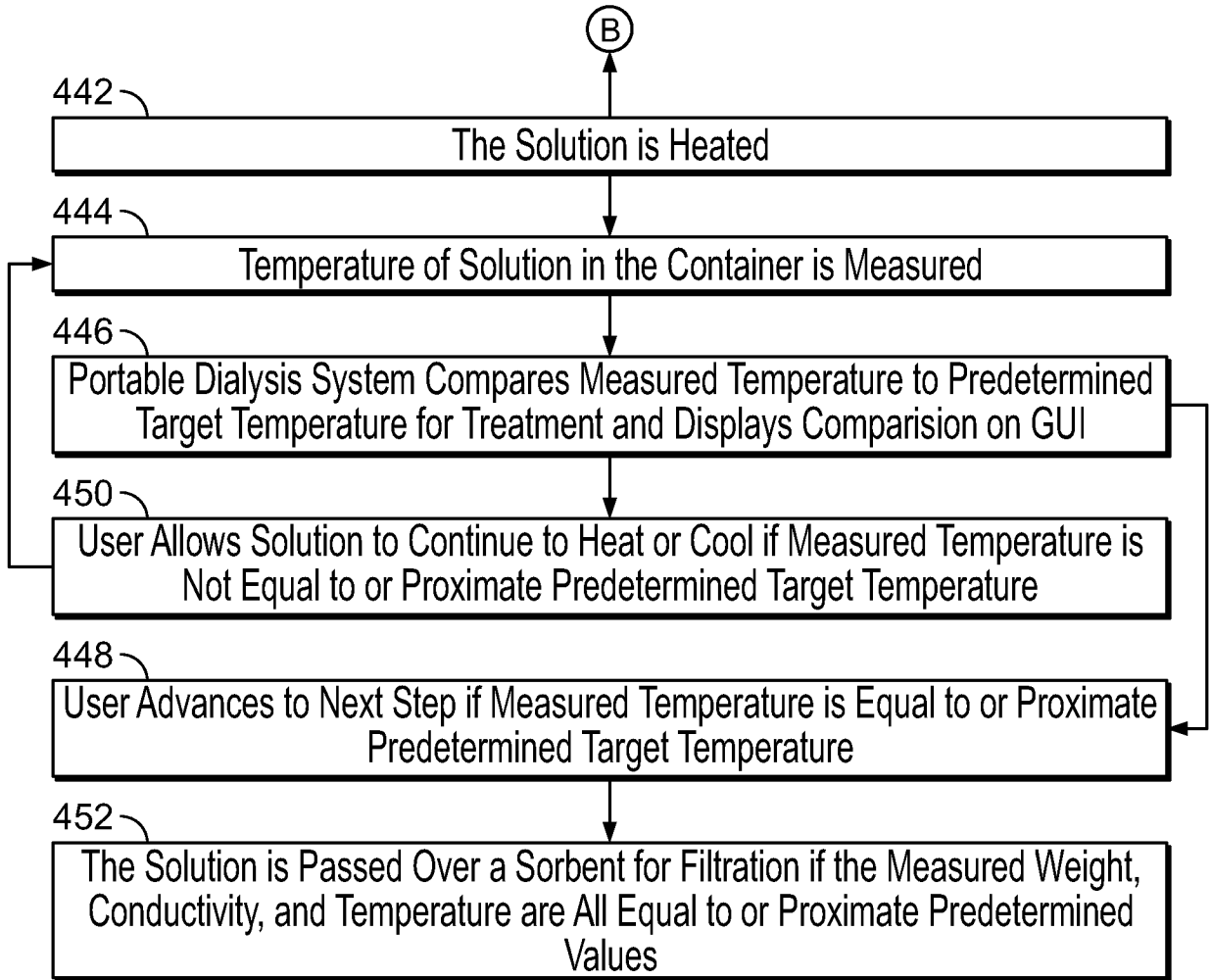


FIG. 4B (Cont.)

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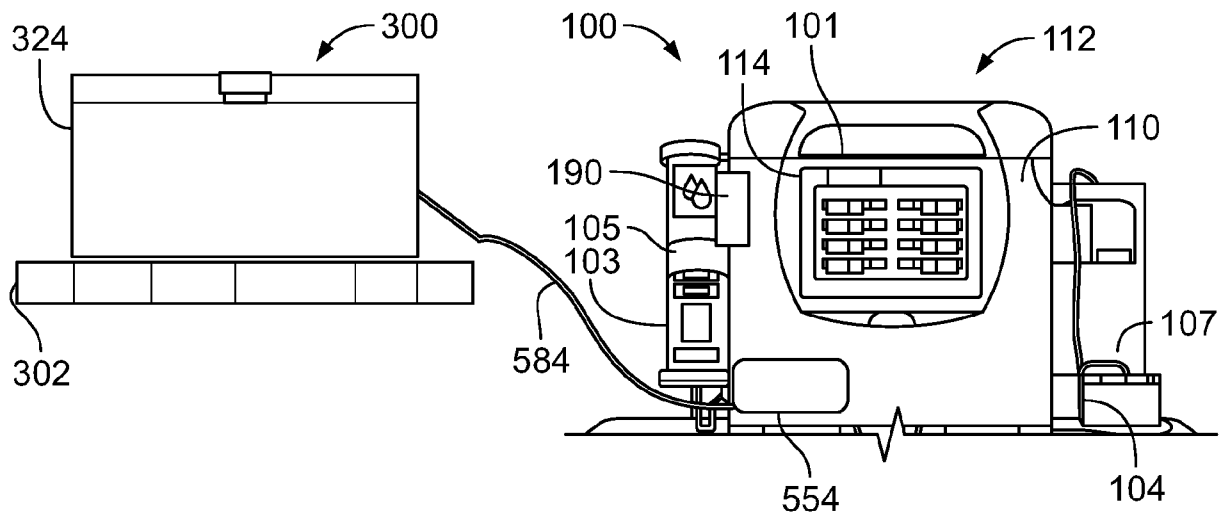


FIG. 5

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 18/25328

A. CLASSIFICATION OF SUBJECT MATTER
 IPC(8) - A61M 1/14, A61M 1/16; A61J 1/16 (2018.01)
 CPC - A61M 1/1605, A61M 1/1621, A61M 1/14, A61M 1/16, A61M 1/1607, A61M 1/1629, A61M 1/1643;
 A61J 1/14, A61J 1/16, A61J 1/18

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

See Search History Document

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

See Search History Document

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

See Search History Document

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	EP 0665026 A2 (Braun Melsungen AG) 20 September 1995 (20.09.1995), Fig. 1, col. 4, ln. 43-55	1-24
A	US 2016/0317733 A1 (Fresenius Medical Care Holdings, Inc.) 03 November 2016 (03.11.2016), Figs. 1-2, 17A, para [0229], [0256]-[0257]	1-24
A	US 2010/0140149 A1 (Fulkerson et al.) 10 June 2010 (10.06.2010), Figs. 1-2, 7a-7b, para [0052], [0086]-[0089]	1-24
A	US 6,045,097 A (Gaffar) 04 April 2000 (04.04.2000), Figs. 1-11, col. 3, ln. 51 - col. 5, ln. 12	1-24
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