



(51) International Patent Classification:

A61K 39/39 (2006.01) B82Y 5/00 (2011.01)
A61K 31/711 (2006.01) C07H 21/04 (2006.01)
A61K 47/10 (2017.01)

(21) International Application Number:

PCT/US2020/036281

(22) International Filing Date:

05 June 2020 (05.06.2020)

(25) Filing Language:

English

(26) Publication Language:

English

(30) Priority Data:

62/858,783 07 June 2019 (07.06.2019) US

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(81) Designated States (unless otherwise indicated, for every kind of national protection available):

AE, AG, AL, AM, AO, AT, AU, AZ, BA, BB, BG, BH, BN, BR, BW, BY, BZ, CA, CH, CL, CN, CO, CR, CU, CZ, DE, DJ, DK, DM, DO, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN, HR, HU, ID, IL, IN, IR, IS, JO, JP, KE, KG, KH, KN, KP, KR, KW, KZ, LA, LC, LK, LR, LS, LU, LY, MA, MD, ME, MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO, NZ, OM, PA, PE, PG, PH, PL, PT, QA, RO, RS, RU, RW, SA, SC, SD, SE, SG, SK, SL, ST, SV, SY, TH, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, WS, ZA, ZM, ZW.

(84) Designated States (unless otherwise indicated, for every kind of regional protection available):

ARIPO (BW, GH, GM, KE, LR, LS, MW, MZ, NA, RW, SD, SL, ST, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, RU, TJ, TM), European (AL, AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV, MC, MK, MT, NL, NO, PL, PT, RO, RS, SE, SI, SK, SM, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, KM, ML, MR, NE, SN, TD, TG).

Published:

- with international search report (Art. 21(3))
- before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments (Rule 48.2(h))

(54) Title: DNA NANOSTRUCTURE-BASED VACCINES

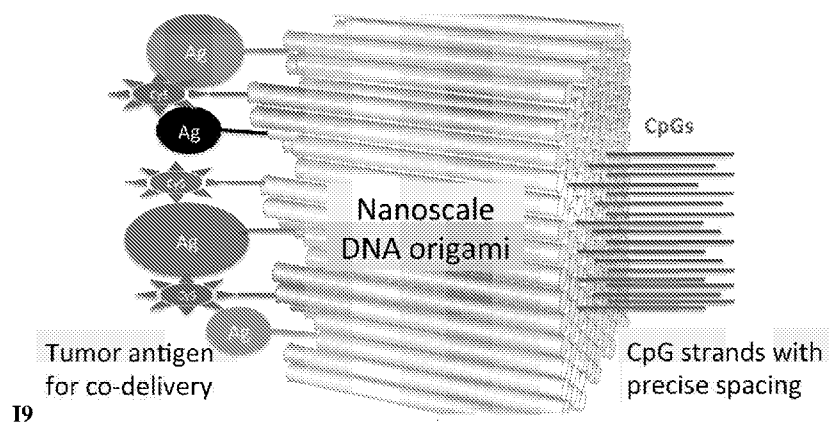


FIG. 1

(57) Abstract: Provided herein, in some embodiments, are nucleic acid nanostructure-based vaccines.



DNA NANOSTRUCTURE-BASED VACCINES

RELATED APPLICATION

This application claims the benefit under 35 U.S.C. § 119(e) of U.S. provisional application number 62/858,783, filed June 7, 2019, which is incorporated by reference herein in its entirety.

BACKGROUND

CpG oligodeoxynucleotides (CpG ODN) that bind toll-like receptor 9 (TLR9) on antigen-presenting cells such as dendritic cells (DCs) have been recognized as promising vaccine adjuvants for effective vaccination (Vaccine 32(48) (2014) 6377). As a result, many DC-based cancer vaccines in development have used CpG ODN in order to induce type 1 (Th1)-polarized immune responses which are associated with cytotoxic T lymphocytes-mediated killing of tumor cells. However, several studies indicated that CpG ODN induced a poorly focused T cell immune response containing both Th1 and Th2 immune responses. CpG spacing at the nanoscale has been known to play important roles in TLR9 activation and subsequent immune polarization to Th1 or Th2 responses (Cell Rep 18(3) (2017) 700).

SUMMARY

Provided herein in various aspects are DNA nanostructure-based vaccines (e.g., cancer vaccines) with an adjuvant (e.g., CpG) spatial distribution that elicits a Th1-polarized immune response. The data provided herein shows (1) that DNA origami—square-lattice blocks (SQBs) with different CpG spacing were successfully fabricated; (2) CpG-Cy5-SQBs prevent DCs from apoptosis and CpG at spacing of 3-5 nm (e.g., 3.5 nm) ('CpG2') showed optimal DC activation in terms of Th1 immune response polarization; and (3) ovalbumin (OVA) conjugated CpG-OVA-SQBs showed superior antigen uptake and CpG at spacing of 3-5 nm (e.g., 3.5 nm) induced an improved Th1 polarized immune response.

Some aspects herein provide CpG-SQBs personalized vaccines (e.g., using multiple antigenic peptides derived from several tumor models).

Some aspects of the present disclosure provide a nucleic acid nanostructure conjugated to an antigen, oligolysine-polyethylene glycol copolymer, and CpG ligand, wherein the CpG ligand is uniformly spaced on the nucleic acid nanostructure.

In some embodiments, the distance between any two adjacent molecules of CpG is 2 nm to 10 nm. For example, the distance between any two adjacent molecules of CpG may be 2-3

nm, 3-4 nm, 4-6 nm, or 6-8 nm. In some embodiments, the distance between any two adjacent molecules of CpG is a 2.5 nm, 3.5 nm, 5 nm, or 7 nm.

In some embodiments, the density of CpG ligand on the nucleic acid nanostructure is 1 molecule of CpG ligand per 5 to 50 nm².

5 In some embodiments, wherein the distance between any two adjacent molecules of CpG is 3.5 nm. Thus, in some embodiments, the density of CpG ligand on the nucleic acid nanostructure is 1 molecule of CpG ligand per 10 to 20 nm².

In some embodiments, the distance between any two adjacent molecules of CpG is 5 nm. Thus, in some embodiments, the density of CpG ligand on the nucleic acid nanostructure is 1
10 molecule of CpG ligand per 20 to 30 nm².

In some embodiments, the nucleic acid nanostructure comprises a two- or three-dimensional square-lattice structure.

In some embodiments, the CpG ligand is located on at least one surface of the nucleic acid nanostructure. In some embodiments, the antigen is located on at least one surface of the
15 nucleic acid nanostructure. In some embodiments, the CpG ligand and the antigen are located on different surfaces of the nucleic acid nanostructure, relative to each other.

In some embodiments, the nucleic acid nanostructure comprises 5 to 25, 10 to 25, or 15 to 25 CpG ligand molecules. In some embodiments, the CpG ligands and/or antigen are located on a single surface of the nucleic acid nanostructure.

20 In some embodiments, the oligolysine-polyethylene glycol (PEG) copolymer comprises ten lysine residues and five PEG molecules (K10PEG5). In some embodiments, the oligolysine-PEG copolymer consists of ten lysine residues and five PEG molecules (K10PEG5).

In some embodiments, the antigen is covalently conjugated to the nanostructure. In some embodiments, the oligolysine-PEG copolymer is covalently conjugated to the nanostructure.

25 In some embodiments, the nucleic acid of the nanostructure comprises DNA, RNA, or a mixture of DNA and RNA. In some embodiments, the nucleic acid of the nanostructure comprises DNA. In some embodiments, the nucleic acid of the nanostructure consists of DNA.

Some aspects of the present disclosure provide a DNA nanostructure conjugated to an antigen, oligolysine-polyethylene glycol copolymer, and CpG ligand, wherein the DNA
30 nanostructure comprises a three-dimensional square-lattice structure, the CpG ligand is uniformly spaced with a density of 1 molecule of CpG ligand per 10-30 nm², and the distance between any two adjacent molecules of CpG is 3-5 nm.

Other aspects of the present disclosure provide a method comprising delivering to a subject the nanostructure of any one of the preceding paragraphs in an effective amount to
35 produce a CD8+ T cell immune response in the subject.

In some embodiments, the subject has a tumor. In some embodiments, the antigen is a tumor antigen.

In some embodiments, administration of the nanostructure results in an at least 2-fold or at least 3-fold reduction in tumor volume.

5 In some embodiments, administration of the nanostructure stimulates cytokine production in dendritic cells of the subject, wherein the cytokine production is at least 10%, at least 15%, or at least 20% higher than cytokine production by dendritic cells in a subject administered antigen only or antigen and free CpG ligand.

10 In some embodiments, administration of the nanostructure stimulates Interleukin-10 (IL10) and/or IL12 production in dendritic cells of the subject.

In some embodiments, administration of the nanostructure increases antigen uptake in dendritic cells of the subject, wherein the antigen uptake is at least 10%, at least 15%, or at least 20% higher than antigen uptake by dendritic cells in a subject administered antigen only or antigen and free CpG ligand.

15 In some embodiments, administration of the nanostructure stimulates a stronger Th1 immune response, relative to stimulation of a Th2 response.

In some embodiments, the Th1 immune response is characterized by expression of CD69 and CD8 on T cells.

20 In some embodiments, administration of the nanostructure stimulates CD8+ T cell proliferation by at least 10%, at least 15%, or at least 20% relative to CD8+ T cell proliferation in control cells in a subject administered antigen only or antigen and free CpG ligand.

25 In some embodiments, administration of the nanostructure stimulates IFN- γ expression in OT-I CD8+ T cells of the subject, wherein the IFN- γ expression is at least 10%, at least 15%, or at least 20% higher than IFN- γ expression by in OT-I CD8+ T cells in a subject administered antigen only or antigen and free CpG ligand.

In some embodiments, administration of the nanostructure increases DC maturation marker expression (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

30 In some embodiments, administration of the nanostructure increases the IL12/IL10 T cell production/secretion ratio (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

In some embodiments, administration of the nanostructure elevates MHC I peptide cross presentation (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

In some embodiments, administration of the nanostructure increases CD8 T cell proliferation (CFSE as an indicator for proliferation and IL-2 secretion) and activation (CD69 and IFN γ secretion) (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

5 In some embodiments, administration of the nanostructure increases CD4 Th1 cell activation (IFN γ) (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

In some embodiments, administration of the nanostructure does not result in an increase in production/proliferation of Treg CD4 cells.

10 In some embodiments, administration of the nanostructure increases CD69 positive T cells *in vivo* in the lymph node (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

In some embodiments, administration of the nanostructure increases CD44 memory T cells *in vivo* in the lymph node (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand)

15 In some embodiments, administration of the nanostructure increases tetramer CD8 T cells *in vivo* (corresponded to cross presentation and CD8 activation) in the lymph node (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

20 In some embodiments, administration of the nanostructure increases infiltrated T cells (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

In some embodiments, administration of the nanostructure increases tetramer CD8 T cells *in vivo* in the tumor (e.g., by at least 10%, at least 20%, at least 30%, at least 40%, or at least 50%) relative to a control (e.g., antigen only or antigen and free CpG ligand).

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic depicting a DNA origami nanostructure as a unique platform for co-delivery of multiple antigens and adjuvant (e.g., CpG) with precise nanoscale distribution.

30 **FIGs. 2A-2E** include data relating to Cadnano design and folding of square-lattice-blocks (SQBs). See Example 1.

FIGs. 3A-3F include data relating to cellular uptake of PEG-purified and K10PEG5-coated CpG-Cy5-SQBs. See Example 2.

FIGs. 4A-4H include data relating to dendritic cell maturation and Th1 immune response polarization. See Example 3.

FIGs. 5A-5F include data relating to antigen uptake and presentation. See Example 4.

FIGs. 6A-6F include data showing that K10PEG5-coated CpG-DNA origami structures stabilize Tregs in the splenocyte while stimulating CD69 expression on CD8 T cells. See Example 5.

5 **FIGs. 7A-7G** includes data showing OT-I and OT-II T cell stimulation *in vitro* and tumor cell killing *in vitro*. See Example 6.

FIGs. 8A-8D show data relating to control spacing for CpG2. See Example 7.

FIGs. 9A-9F show data relating to therapeutic and prophylactic effects in a mouse melanoma tumor model. See Example 8.

10 **FIGs. 10A-10M** show data relating to immune cell profiling in animals post vaccination. See Example 9.

DETAILED DESCRIPTION

In some aspects, the present disclosure provides a nucleic acid (e.g., DNA) nanostructure comprising a plurality (e.g., 10, 20, 50, 100, 1000, 10,000, 10-20, 10-50, 10-100, 10-1000, 10-1000, 100-1000, 100-10000, or 1000-10000) of uniformly spaced CpG ligands and a plurality (e.g., 10, 20, 50, 100, 1000, 10,000, 10-100, 10-1000, 10-1000, 100-1000, 100-10000, or 1000-10000) of antigens, wherein the nucleic acid nanostructure is coated and covalently crosslinked with oligolysine-polyethylene glycol (PEG) copolymer.

20 In some embodiments, a nucleic acid nanostructure comprises at least 5, at least 10, or at least 20 adjuvant (e.g., CpG ligand) molecules. In some embodiments, a nucleic acid nanostructure comprises at least 5 but less than 65 adjuvant (e.g., CpG ligand) molecules. For example, a nucleic acid nanostructure may comprise 5-55, 5-50, 5-45, 5-40, 5-35, 5-30, 5-35, 5-20, 10-55, 10-50, 10-45, 10-40, 10-35, 10-30, 10-35, 10-20, 15-55, 15-50, 15-45, 15-40, 15-35, 25 15-30, 15-35, or 15-20 adjuvant (e.g., CpG ligand) molecules. In some embodiments, the nucleic acid nanostructure comprises 5 to 25, 10 to 25, or 15 to 25 adjuvant (e.g., CpG ligand) molecules. In some embodiments, a nucleic acid nanostructure comprises 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, or 20 adjuvant (e.g., CpG ligand) molecules. In some embodiments, a nucleic acid nanostructure comprises 18 adjuvant (e.g., CpG ligand) molecules.

30 In some embodiments, each CpG ligand of the plurality of CpG ligands is uniformly spaced 2.0 nm, 2.5 nm, 3.0 nm, 3.5 nm, 4.0 nm, 4.5 nm, 5 nm, 5.5 nm, 6 nm, 6.5 nm, or 7 nm from any other adjacent CpG ligand. In some embodiments, each CpG ligand of the plurality of CpG ligands is uniformly spaced 3.5 nm from any other adjacent CpG ligand. In some embodiments, each CpG ligand of the plurality of CpG ligands is uniformly spaced 5 nm from any other adjacent CpG ligand. In some embodiments, each CpG ligand of the plurality of CpG

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ligands is uniformly spaced 2 nm-10 nm, 2.5 nm-10 nm, 3 nm-10 nm, 3.5 nm-10 nm, 4 nm-10 nm, 4.5 nm-10 nm, 5 nm-10 nm, 5.5 nm-10 nm, 6 nm-10 nm, 6.5 nm-10 nm, 7 nm-10 nm, 7.5 nm-10 nm, 8 nm-10 nm, 8.5 nm-10 nm, 9 nm-10 nm, 9.5 nm-10 nm from any other adjacent CpG ligand.

5 In some aspects, the present disclosure provides a nucleic acid nanostructure comprising a plurality of CpG ligands and a plurality of antigens, wherein each CpG ligand of the plurality of CpG ligands is uniformly spaced 3.5 nm from any other CpG ligand.

In some embodiments, the distance between any two adjacent molecules of adjuvant (e.g., CpG ligand) is 2 nm-10 nm. For example, the distance between any two adjacent
10 molecules of adjuvant (e.g., CpG ligand) may be 2-3 nm, 3-4 nm, 4-6 nm, or 6-8 nm. In some embodiments, the distance between any two adjacent molecules of adjuvant (e.g., CpG ligand) is a 2.5 nm, 3.5 nm, 5 nm, or 7 nm. Uniform spacing herein refers to the distance between any two adjacent molecules, measuring from the center of the molecule. With reference to FIG. 2E, for example, the outlined circles represent individual CpG ligands, and the distance between the
15 center of two adjacent CpG ligands is 2.5 nm, 3.5 nm, 5 nm, and 7 nm, top to bottom images, respectively.

In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 5 to 50 nm².

In some embodiments, the distance between any two adjacent molecules of adjuvant
20 (e.g., CpG ligand) is 2.5 nm. In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 5 to 10 nm². In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 5, 5.5, 6, 6.5, 7, 7.5, 8, 8.5, 9, 9.5, or 10 nm².

In some embodiments, the distance between any two adjacent molecules of adjuvant
25 (e.g., CpG ligand) is 3.5 nm. In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 10 to 20 nm². For example, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure may be 10 to 15 nm². In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 10, 10.5, 11, 11.5, 12, 12.5, 13,
30 13.5, 14, 14.5, or 15 nm².

In some embodiments, the distance between any two adjacent molecules of adjuvant (e.g., CpG ligand) is 5 nm. In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 20 to 30 nm². In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure

is 1 molecule of adjuvant (e.g., CpG ligand) per 20, 20.5, 21, 21.5, 22, 22.5, 23, 23.5, 24, 24.5, 25, 25.5, 26, 26.5, 27, 27.5, 28, 28.5, 29, 29.5, or 30 nm².

In some embodiments, the distance between any two adjacent molecules of adjuvant (e.g., CpG ligand) is 7 nm. In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 45 to 55 nm². In some embodiments, the density of adjuvant (e.g., CpG ligand) on the nucleic acid nanostructure is 1 molecule of adjuvant (e.g., CpG ligand) per 45, 45.5, 46, 46.5, 47, 47.5, 48, 48.5, 49, 49.5, 50, 50.5, 51, 51.5, 52, 52.5, 53, 53.5, 54, 54.5, or 55 nm².

In some embodiments, the nucleic acid nanostructure is coated and covalently crosslinked with oligolysine-polyethylene glycol (PEG) copolymer.

In some embodiments, the nucleic acid nanostructure is a nucleic acid (e.g., DNA) origami nanostructure. In some embodiments, the nucleic acid (e.g., DNA) origami nanostructure is a 126-helix nucleic acid (e.g., DNA) origami nanostructure. In some embodiments, the nucleic acid nanostructure is a nucleic acid (e.g., DNA) single-stranded tile (SST) nanostructure.

In some embodiments, the plurality of antigens comprise ovalbumin.

In some embodiments, the plurality of antigens are covalently linked to the nanostructure. In some embodiments, the plurality of antigens are covalently linked to free amine groups of the nucleic acid nanostructure.

In some aspects, the present disclosure provides a method of inducing a Th1 polarized immune response in cells, the method comprising administering to a subject (e.g., a human subject) the nucleic acid nanostructure provided herein.

In some aspects, the present disclosure provides a method of inducing a Th1 polarized immune response in cells, the method comprising administering to a subject a nucleic acid nanostructure comprising a plurality of uniformly spaced CpG ligands and a plurality of antigens.

In some embodiments, the volume of the tumor is reduced at least 2-fold, at least 3-fold, at least 4-fold, at least 5-fold, relative to control (e.g., wherein the control is free CpG + free antigen + free nanostructure, or wherein the control is buffer only). In some embodiments, the volume of the tumor is reduced 2-fold, 3-fold, 4-fold, or 5-fold relative to control.

In some embodiments, the nucleic acid nanostructure is administered to the subject multiple times (e.g., at least 2 times, at least 3 times, etc.).

Oligolysine-polyethylene glycol (PEG) copolymer

Aspects of the present disclosure provide nucleic acid nanostructures covalently coated with oligolysine-PEG copolymer (oligolysine comprising lysine amino acids and PEG moieties) that protect the nanostructures from degradation, for example, under physiological conditions of magnesium and/or calcium depletion and nuclease activity. Nucleic acid nanostructures, in general, typically require up to 16 mM magnesium ion (Mg^{2+}) to neutralize electrostatic repulsion and thereby stabilize their shape. Thus, such structures exhibit poor structural integrity in biological buffers (*e.g.*, buffers containing physiological levels of Mg^{2+} (*e.g.*, 0.6 mM) and Ca^{2+} (*e.g.*, 1.2 mM)). Further, the activity of DNase I in freshly prepared cell medium containing 10% fetal bovine serum, which is typically used in biomedical applications, causes rapid degradation of nucleic acid nanostructures. The structural integrity of nucleic acid nanostructures can be maintained, even under physiological conditions (*e.g.*, including low salt conditions), by linking the nanostructures to positively charged oligolysine (*e.g.*, oligolysine-PEG copolymer), which neutralize electrostatic repulsion and enhance nucleic acid resistance to nuclease degradation, thereby stabilizing the shape of the nanostructures.

Nucleic acid nanostructures may be covalently coated with oligolysine-PEG copolymer such that the covalent crosslink occurs between an oligolysine-PEG copolymer and the nucleic acid nanostructure involves the amine of a lysine amino acid side chain of the polylysine polymer. The covalent crosslink may be formed using an aldehyde crosslinking agent or any suitable crosslinking agent. In some embodiments, an aldehyde crosslinking agent is formaldehyde or glutaraldehyde.

Nucleic acid nanostructures may be covalently coated with oligolysine such that the covalent crosslink occurs between any atom of an oligolysine and any atom of the nucleic acid nanostructure. In some embodiments, the covalent crosslink is formed using a nucleic acid crosslinking agent. In some embodiments, a nucleic acid crosslinking agent is cisplatin or methoxypsoralen (8-MOP).

Oligolysine-PEG copolymer of the present invention is a cationic polymer, which, without being bound by any particular theory, may be used to shield the negatively charged phosphate backbone of nucleic acids, thereby promoting close packing of nucleic acid helices to stabilize the shape of and slow down nuclease degradation of the nanostructures.

Oligolysine-PEG copolymer may comprise any one or more functional groups in addition to its primary amine groups. As used herein, a "functional group" refers to an atom or group of atoms, such as a carboxyl group, that replaces hydrogen in an organic compound and determines the chemical behavior of the compound. Examples of common functional groups include, without limitation, alkane, ether, ketone, alkene, aldehyde, alkyne, imine, carboxylic acid, alkyl

halide, ester, alcohol, thioester, thiol, amide, acyl phosphate, acid chloride, thioether, phosphate monoester, phenol and phosphate diester. Oligolysine of the present disclosure include linear, branched and dendrimer polymers. Oligolysine of the present disclosure, in some embodiments, are not limited by length of the polymer.

5 The length of oligolysine-PEG copolymer may vary. In some embodiments, the length of an oligolysine is 5-100 lysines (i.e., the oligolysine comprise 5-100 lysines). For example, the length of an oligolysine may be 5-75, 5-50, 5-25, 5-20, 5-25, or 5-10 lysines. In some embodiments, the length of an oligolysine is 5, 10, 15, 20, 25, 30, 35, 40, 45, 50, 55, 60, 65, 70, 75, 80, 85, 90, 95, or 100 lysines.

10 In some embodiments, an oligolysine-PEG copolymer includes one or more additional amino acids (*e.g.*, alanine, arginine, asparagine, aspartic acid, cysteine, glutamine, glutamic acid, glycine, histidine, isoleucine, leucine, lysine, methionine, phenylalanine, proline, serine, threonine, tryptophan, tyrosine, valine) and/or analogs thereof. Thus, oligolysine may comprise or consist of peptides (*e.g.*, short chains of amino acid monomers linked by peptide (*e.g.*, amide) 15 bonds). In some embodiments, oligolysine-PEG copolymer comprise positively charged amino acids such as lysine and/or arginine. In some embodiments, the oligolysine-PEG copolymer may comprise poly-L-lysine polymers.

In some embodiments, an oligolysine-PEG copolymer comprises a plurality of lysines. In some embodiments, an oligolysine-PEG copolymer comprises at least 10%, at least 15%, at least 20 20%, at least 25%, at least 30%, at least 35%, at least 40%, at least 45%, at least 50%, at least 55%, at least 60%, at least 65%, at least 70%, at least 75%, at least 80%, at least 85%, at least 90%, at least 95%, or 100% lysine amino acids. In some embodiments, a region of amino acids comprises 50% to 100%, 55% to 100%, 60% to 100%, 65% to 100%, 70% to 100%, 75% to 100%, 80% to 100%, 85% to 100% or 90% to 100% lysine amino acids.

25 Lysines of oligolysine-PEG copolymer, in some embodiments, are separated from each other by at least 1, at least 2, at least 3, at least 4, at least 5, at least 6, at least 7, at least 8, at least 9, at least 10 or more, non-amine containing amino acids such as non-lysine amino acids. In some embodiments, lysines of oligolysine-PEG copolymer are separated from each other by 1 to 5, or 1 to 10, non-amine containing amino acids such as non-lysine amino acids. In some 30 embodiments, lysines of oligolysine-PEG copolymer are regularly spaced. The following are non-limiting examples of linear oligolysine having regularly-spaced lysine (K), where X is a non-lysine amino acid, or functional group, and n is any integer equal to or greater than 1:

- (i) $K-X-(K-X)_n-K$, or $X-(K-X)_n$, $K-X-(K-X)_n$, or $X-(K-X)_n-K$;
 (ii) $K-X-X-(K-X-X)_n-K$, or $X-X-(K-X-X)_n$, or $K-X-X-(K-X-X)_n$, or
 35 $X-X-(K-X-X)_n-K$; or

(iii) $K-X-X-X-(K-X-X-X)_n-K$, or $X-X-X-(K-X-X-X)_n$, or $K-X-X-X-(K-X-X-X)_n$, or $X-X-X-(K-X-X-X)_n-K$.

In some embodiments, the oligolysine herein comprise a polyethylene glycol (PEG) moiety or a related ether-containing functional group. A PEG moiety may comprise at least 5, at least 10, at least 25, at least 50, at least 75, at least 100, at least 125, at least 150, at least 175, at least 200, at least 250, at least 300, at least 350, at least 400, at least 450, at least 500, at least 550, at least 600, at least 650, at least 700, at least 750, at least 800, at least 850, at least 900, at least 950, at least 1000, at least 1250, at least 1500, or at least 2000 polyethylene glycol monomer units. In some embodiments, a PEG moiety may comprise 5-100, 50-100, 50-200, 100-200, 100-150, 200-250, 200-300, 250-500, 400-600, 500-1000, 750-1000, 750-1500, or 1250-2000 polyethylene glycol monomer units. In some embodiments, a PEG moiety is PEG 1K (average molecular weight of 1000 Daltons), PEG 5K (average molecular weight of 5000 Daltons), PEG 10K (average molecular weight of 10000 Daltons), PEG 20K (average molecular weight of 20000 Daltons), PEG 25K (average molecular weight of 25000 Daltons), PEG 50K (average molecular weight of 50000 Daltons), or PEG 100K (average molecular weight of 100000 Daltons).

Nucleic Acid Nanostructures

A “nucleic acid nanostructure,” as used herein, refers to nucleic acids that form (*e.g.*, self-assemble) two-dimensional (2D) or three-dimensional (3D) shapes (*e.g.*, reviewed in W.M. Shih, C. Lin, *Curr. Opin. Struct. Biol.* 20, 276 (2010), incorporated by reference herein). Nanostructures may be formed using any nucleic acid folding or hybridization methodology. One such methodology is DNA origami (*see, e.g.*, Rothmund, P.W.K. *Nature* 440 (7082): 297-302 (2006), incorporated by reference herein). In a DNA origami approach, a nanostructure is produced by the folding of a longer “scaffold” nucleic acid strand through its hybridization to a plurality of shorter “staple” oligonucleotides, each of which hybridize to two or more non-contiguous regions within the scaffold strand. In some embodiments, a scaffold strand is at least 100 nucleotides in length. In some embodiments, a scaffold strand is at least 500, at least 1000, at least 2000, at least 3000, at least 4000, at least 5000, at least 6000, at least 7000, or at least 8000 nucleotides in length. The scaffold strand may be naturally or non-naturally occurring. Staple strands are typically less than 100 nucleotides in length; however, they may be longer or shorter depending on the application and depending upon the length of the scaffold strand. In some embodiments, a staple strand may be 15 to 100 nucleotides in length. In some embodiments, a staple strand is 25 to 50 nucleotides in length.

In some embodiments, a nucleic acid nanostructure may be assembled in the absence of a scaffold strand (*e.g.*, a scaffold-free structure). For example, a number of oligonucleotides (*e.g.*, less than 200 nucleotides or less than 100 nucleotides in length) may be assembled to form a nucleic acid nanostructure.

5 Other methods for assembling nucleic acid nanostructures are known in the art, any one of which may be used herein. Such methods are described by, for example, Bellot G. *et al.*, *Nature Methods*, 8: 192-194 (2011); Liedl T. *et al.*, *Nature Nanotechnology*, 5: 520-524 (2010); Shih W.M. *et al.*, *Curr. Opin. Struct. Biol.*, 20: 276-282 (2010); Ke Y. *et al.*, *J. Am. Chem. Soc.*, 131: 15903-08 (2009); Dietz H. *et al.*, *Science*, 325: 725-30 (2009); Hogberg B. *et al.*, *J. Am.*
10 *Chem. Soc.*, 131: 9154-55 (2009); Douglas S.M. *et al.*, *Nature*, 459: 414-418 (2009); Jungmann R. *et al.*, *J. Am. Chem. Soc.*, 130: 10062-63 (2008); Shih W.M., *Nature Materials*, 7: 98-100 (2008); and Shih W.M., *Nature*, All: 618-21 (2004), each of which is incorporated herein by reference in its entirety.

A nucleic acid nanostructure may be assembled into one of many defined and
15 predetermined shapes including without limitation a capsule, hemi-sphere, a cube, a cuboidal, a tetrahedron, a cylinder, a cone, an octahedron, a prism, a sphere, a pyramid, a dodecahedron, a tube, an irregular shape, and an abstract shape. The nanostructure may have a void volume (*e.g.*, it may be partially or wholly hollow). In some embodiments, the void volume may be at least 25%, at least 50%, at least 75%, at least 85%, at least 90%, or more of the volume of the
20 nanostructure. Thus, in some embodiments, nucleic acid nanostructures do not comprise a solid core. In some embodiments, nucleic acid nanostructures are not circular or near circular in shape. In some embodiments, nucleic acid nanostructures are not a solid core sphere. Depending on the intended use, nucleic acid nanostructures may be assembled into a shape as simple as a two-dimensional sheet or as complex as a three-dimensional capsule or lattice (or even more
25 complex).

In some embodiments, the nucleic acid nanostructure comprises a two- or three-dimensional square-lattice structure. A description of three-dimensional square-lattice structure is described in Yonggang Ke *et al.*, *Multilayer DNA Origami Packed on a Square Lattice*. *J Am Chem Soc.* 2009 Nov 4;131(43):15903-8, incorporated herein in its entirety.

30 Nucleic acid nanostructures may be made of, or comprise, DNA, RNA, modified DNA, modified RNA, PNA, LNA or a combination thereof.

In some embodiments, nucleic acid nanostructures are rationally designed. A nucleic acid nanostructure is herein considered to be “rationally designed” if nucleic acids that form the nanostructure are selected based on pre-determined, predictable nucleotide base pairing
35 interactions that direct nucleic acid hybridization. For example, nucleic acid nanostructures may

be designed prior to their synthesis, and their size, shape, complexity and modification may be prescribed and controlled using certain select nucleotides (*e.g.*, oligonucleotides) in the synthesis process. The location of each nucleic acid in the structure may be known and provided for before synthesizing a nanostructure of a particular shape. The fundamental principle for designing, for example, self-assembled nucleic acid nanostructures is that sequence complementarity in nucleic acid strands is selected such that, by pairing up complementary segments, the nucleic acid strands self-organize into a predefined nanostructure under appropriate physical conditions. Thus, in some embodiments, nucleic acid nanostructures are self-assembling. Similarly, handles and anti-handle nucleic acids (*e.g.*, those linked to adjuvant and/or antigen) may be rationally designed to attach specifically to an interior or exterior surface of a nanostructure, in some embodiments, without intercalation or hybridization with nucleic acids forming the body of the nanostructure.

Examples of nucleic acid nanostructures for use in accordance with the present disclosure include, without limitation, capsules, lattices (E. Winfree, et al. *Nature* 394, 539 (1998); H. Yan, et al. *Science* 301, 1882 (2003); H. Yan, et al. *Proc. Natl. Acad. of Sci. USA* 100, 8103 (2003); D. Liu, et al. *J. Am. Chem. Soc.* 126, 2324 (2004); P.W.K. Rothmund, et al. *PLoS Biology* 2, 2041 (2004)), ribbons (S.H. Park, et al. *Nano Lett.* 5, 729 (2005); P. Yin, et al. *Science* 321, 824 (2008)), tubes (H. Yan *Science* (2003); P. Yin (2008)), finite two-dimensional (2D) and three dimensional (3D) objects with defined shapes (J. Chen, N. C. Seeman, *Nature* 350, 631 (1991); P. W. K. Rothmund, *Nature* 440, 297 (2006); Y. He, et al. *Nature* 452, 198 (2008); Y. Ke, et al. *Nano. Lett.* 9, 2445 (2009); S. M. Douglas, et al. *Nature* 459, 414 (2009); H. Dietz, et al. *Science* 325, 725 (2009); E. S. Andersen, et al. *Nature* 459, 73 (2009); T. Liedl, et al. *Nature Nanotech.* 5, 520 (2010); D. Han, et al. *Science* 332, 342 (2011)), and macroscopic crystals (J. P. Meng, et al. *Nature* 461, 74 (2009)). Other nucleic acid nanostructures may be used as provided herein.

Cadnano software may be used to design particular nucleic acid nanostructures of interest (*see* cadnano.org).

Polylysine, a cationic polymer, is known to be efficient in condensing plasmid DNA into compact particles, for example, for delivery of therapeutic DNA. DNA is a highly negatively charged polymer due to the repeating phosphate groups along the polymer backbone. The interaction with cationic polymers such as polylysine is therefore an electrostatic one. It is generally accepted that DNA condensation occurs through neutralization of negative charges on the DNA by its interactions with cationic oligolysine, followed by hydrophobic collapse as water is displaced from the DNA structure. Generally, DNA is super-saturated with oligolysine such that most or all of the negative charges of the DNA are neutralized, and the DNA condenses into a compact particle of 12 nm to 300 nm in diameter, depending on the weight of the polylysine

polymer and the condensation conditions (*e.g.*, charge ratio between polymer and DNA, salt concentration and temperature). In some embodiments, the term “condensed nucleic acid” refers to a nucleic acid particle that has a diameter and/or volume that is less than 80%, less than 70%, less than 60%, less than 50%, or less than 40% of the diameter and/or volume of its non-
5 condensed state (*e.g.*, without being supersaturated with polylysine). Unlike the condensed, compacted DNA particles described above, the nucleic acid nanostructures of the present disclosure are not condensed into compact particles when complexed with oligolysine in accordance with the present disclosure. Rather, nucleic acid nanostructures provided herein maintain their structure integrity. In some embodiments, the nucleic acid nanostructures are
10 “subsaturated” or “saturated” with covalently linked oligolysine (*e.g.*, coated with oligolysine at a N:P (nitrogen in lysine to phosphorus in nucleic acid) ratio of 0.1:1 to 1:1) such that the architecture of the structures is not compromised. That is, nucleic acid nanostructures of the present disclosure have a 2D or 3D shape, despite the additional weight of and covalent interactions with positively-charged oligolysine.

15 Thus, nucleic acid nanostructures provided herein, in some embodiments, are subsaturated with oligolysine-PEG copolymer (*e.g.*, coated with oligolysine-PEG copolymer at a N:P (nitrogen in lysine to phosphorus in nucleic acid) ratio of 0.1:1 to 0.95:1). As discussed above, nucleic acid nanostructures are considered to be “subsaturated” with oligolysine-PEG copolymer if less than 100% of the phosphates of the nucleic acid nanostructure backbone are
20 linked to amines of oligolysine-PEG copolymer. In some embodiments, less than 98%, less than 95%, less than 90%, less than 85%, less than 80%, less than 75%, less than 70%, less than 65%, less than 60%, less than 55%, less than 50%, less than 45%, less than 40%, less than 35%, less than 30%, less than 25%, less than 20%, less than 15% or less than 10% of the phosphates of nucleic acid nanostructure are linked to amines of the oligolysine-PEG copolymer. In some
25 embodiments, 10% to 90%, 10% to 80%, 10% to 50%, 20% to 90%, or 20% to 80% of the phosphates of the nucleic acid nanostructure backbone are linked to amines of oligolysine-PEG copolymer. Further, as discussed above, nucleic acid nanostructures are considered to be “subsaturated” with oligolysine-PEG copolymer if, nanostructures are coated with oligolysine-PEG copolymer at a N:P ratio of 0.1:1, 0.2:1, 0.3:1, 0.4:1, 0.5:1, 0.6:1, 0.7:1, 0.8:1, 0.9:1, or
30 0.95:1. In some embodiments, nucleic acid nanostructures provided herein are saturated with oligolysine-PEG copolymer (*e.g.*, coated with oligolysine at a N:P (nitrogen in lysine to phosphorus in nucleic acid) ratio of 1:1). Thus, in some embodiments, nanostructures are coated with oligolysine-PEG copolymer at a N:P ratio of 0.1:1 to 1:1, 0.2 to 1:1, 0.3 to 1:1, 0.5 to 1:1, 0.75:1:1, 0.9:1 to 1:1, 0.95:1 to 1:10.1:1 to 0.95:1, 0.2:1 to 0.95:1, 0.5:1 to 0.95:1, 0.1:1 to 0.3:1,
35 0.2:1 to 0.4:1, 0.4:1 to 0.5:1, 0.5:1 to 0.75:1, 0.5:1 to 0.8:1, 0.6:1 to 0.8:1, 0.7:1 to 0.95:1, 0.8:1

to 0.95:1, or 0.9:1 to 0.95:1. At such subsaturated or saturated levels, nucleic acid nanostructures still maintain their structural integrity (*e.g.*, keep their original shape), despite their interactions with oligolysine-PEG copolymer. It should be understood that a nucleic acid nanostructure coated in oligolysine-PEG copolymer is herein considered to “maintain its structural integrity” if the shape of the nanostructure, under the same environmental conditions, can be distinguished/discerned for a period of time that is greater than that of a control nucleic acid nanostructure (*e.g.*, a similar nucleic acid nanostructure that is not coated with oligolysine-PEG copolymer).

Surprisingly, nucleic acid nanostructures that are covalently linked to oligolysine-PEG copolymer as described herein are even more structurally stable and are more resistant to degradation (*e.g.*, at low and/or physiological salt concentrations, in presence of nucleases) than nanostructures that are non-covalently linked to oligolysine-PEG copolymer. In some embodiments, nucleic acid nanostructures that are covalently linked to oligolysine-PEG copolymer are at least 2-fold, at least 5-fold, at least 10-fold, at least 20-fold, at least 50-fold, at least 100-fold, at least 150-fold, at least 180-fold, or at least 200-fold more resistant to degradation (*e.g.*, nuclease degradation, *e.g.*, in the presence of DNaseI nuclease) than nanostructures that are non-covalently linked to oligolysine-PEG copolymer.

The relationship between amines of oligolysine-PEG copolymer and phosphates of nucleic acid nanostructures may be described in terms of an amine to phosphate ratio. The “N/P ratio,” herein, refers to the ratio of positive (+) charges contributed to a structure by a primary, secondary or tertiary amine that can be protonated (*e.g.*, in the side chain of a lysine) to negative (-) charges contributed to a nanostructure by phosphates of its nucleic acid backbone. For example, lysine in the middle of a peptide contributes 1 + charge, while lysine at the N-terminus of a peptide contributes 2 + charges. Thus, “subsaturated,” refers to a N:P ratio of 0.95:1 or lower (*i.e.*, lower number of amines compared to phosphates). “Saturated,” by comparison, refers to a N:P ratio of 1:1 (*i.e.*, the same number of amine compared to phosphates). “Supersaturated” refers to a N:P ratio of 1.05:1 or greater (*i.e.*, greater number of amines compared to phosphates). Thus, in some embodiments, the ratio of amines or amines to phosphate (*e.g.*, amines of oligolysine-PEG copolymer that interact with (*e.g.*, are linked to) phosphates of a nucleic acid nanostructure backbone) is lower than 1:1. For example, the ratio of amines phosphates may be 0.9:1, 0.8:1, 0.7:1, 0.6:1, 0.5:1, 0.4:1, 0.3:1, 0.2:1 or 0.1:1. In some embodiments, the ratio of amines to phosphates is 0.9:1 to 0.1:1, 0.9:1 to 5:1, 0.8:1 to 0.1:1 or 0.5:1 to 0.1:1. In some embodiments, the ratio of amines to phosphates is 1:1.

In some embodiments, the ratio of amines or amine to phosphate (*e.g.*, amine of oligolysine-PEG copolymer that interact with (*e.g.*, are linked to) phosphates of a nucleic acid nanostructure backbone) is 1:1.

As used herein, the terms “nucleic acid” and/or “oligonucleotide” may refer to at least
5 two nucleotides covalently linked together. A nucleic acid of the present disclosure may generally contain phosphodiester bonds, although in some cases, nucleic acid analogs are included that may have other backbones, comprising, for example, phosphoramidite (Beaucage et al., *Tetrahedron* 49(10):1925 (1993) and references therein; Letsinger, *J. Org. Chem.* 35:3800 (1970); Sprinzl et al., *Eur. J. Biochem.* 81:579 (1977); Letsinger et al., *Nucl. Acids Res.* 14:3487
10 (1986); Sawai et al., *Chem. Lett.* 805 (1984), Letsinger et al., *J. Am. Chem. Soc.* 110:4470 (1988); and Pauwels et al., *Chemica Scripta* 26:141 (1986)), phosphorothioate (Mag et al., *Nucleic Acids Res.* 19:1437 (1991); and U.S. Pat. No. 5,644,048), phosphorodithioate (Briu et al., *J. Am. Chem. Soc.* 111:2321 (1989), O-methylphosphoroamidite linkages (see Eckstein, *Oligonucleotides and Analogues: A Practical Approach*, Oxford University Press), and peptide nucleic acid backbones
15 and linkages (see Egholm, *J. Am. Chem. Soc.* 114:1895 (1992); Meier et al., *Chem. Int. Ed. Engl.* 31:1008 (1992); Nielsen, *Nature*, 365:566 (1993); Carlsson et al., *Nature* 380:207 (1996), all of which are incorporated by reference). Other analog nucleic acids include those with positive backbones (Denpcy et al., *Proc. Natl. Acad. Sci. USA* 92:6097 (1995); non-ionic backbones (U.S. Pat. Nos. 5,386,023, 5,637,684, 5,602,240, 5,216,141 and 4,469,863; Kiedrowshi et al.,
20 *Angew. Chem. Intl. Ed. English* 30:423 (1991); Letsinger et al., *J. Am. Chem. Soc.* 110:4470 (1988); Letsinger et al., *Nucleoside & Nucleotide* 13:1597 (1994); Chapters 2 and 3, ASC Symposium Series 580, "Carbohydrate Modifications in Antisense Research", Ed. Y. S. Sanghui and P. Dan Cook; Mesmaeker et al., *Bioorganic & Medicinal Chem. Lett.* 4:395 (1994); Jeffs et al., *J. Biomolecular NMR* 34:17 (1994); *Tetrahedron Lett.* 37:743 (1996)) and non-ribose
25 backbones, including those described in U.S. Pat. Nos. 5,235,033 and 5,034,506, and Chapters 6 and 7, ASC Symposium Series 580, "Carbohydrate Modifications in Antisense Research", Ed. Y. S. Sanghui and P. Dan Cook. Nucleic acids containing one or more carbocyclic sugars are also included within the definition of nucleic acids (see Jenkins et al., *Chem. Soc. Rev.* (1995) pp169-176). Several nucleic acid analogs are described in Rawls, *C & E News* Jun. 2, 1997 page 35. All
30 of these references are hereby expressly incorporated by reference. Nucleic acid may have a homogenous backbone (*e.g.*, entirely phosphodiester or entirely phosphorothioate) or a heterogeneous (or chimeric) backbone. Phosphorothioate backbone modifications render a nucleic acid less susceptible to nucleases and thus more stable (as compared to a native phosphodiester backbone nucleic acid) under certain conditions. Other linkages that may provide
35 more stability to a nucleic acid include without limitation phosphorodithioate linkages,

methylphosphonate linkages, methylphosphorothioate linkages, boranophosphonate linkages, peptide linkages, alkyl linkages, dephospho type linkages, and the like. Thus, in some instances, nucleic acids have non-naturally occurring backbones. Modifications of the ribose-phosphate backbone may be done, for example, to facilitate the addition of labels, or to increase the stability and half-life of such molecules in physiological environments.

Nucleic acids may be single-stranded (ss) or double-stranded (ds), as specified, or may contain portions of both single-stranded and double-stranded sequence (*e.g.*, are partially double-stranded). Nucleic acids may be DNA, both genomic and cDNA, RNA or a hybrid, where the nucleic acid contains any combination of deoxyribo- and ribonucleotides, and any combination of bases, including uracil, adenine, thymine, cytosine, guanine, inosine, xanthine hypoxanthine, isocytosine, and isoguanine. As used herein, the term “nucleoside” includes nucleotides as well as nucleoside and nucleotide analogs, and modified nucleosides such as amino modified nucleosides. In addition, “nucleoside” includes non-naturally occurring analog structures. Thus, for example, the individual units of a peptide nucleic acid, each containing a base, are referred to herein as a nucleoside.

Nucleic acids include DNA such as B-form DNA, D-form DNA and L-form DNA and RNA, as well as various modifications thereof. Modifications include base modifications, sugar modifications, and backbone modifications. Non-limiting examples of these are provided below.

Non-limiting examples of DNA variants that may be used as provided herein are L-DNA (the backbone enantiomer of DNA, known in the literature), peptide nucleic acids (PNA) bisPNA clamp, a pseudocomplementary PNA, a locked nucleic acid (LNA), or co-nucleic acids of the above such as DNA-LNA co-nucleic acids. It is to be understood that nucleic acids used as provided herein may be homogeneous or heterogeneous in nature. As an example, they may be completely DNA in nature or they may comprise DNA and non-DNA (*e.g.*, LNA) monomers or sequences. Thus, any combination of nucleic acid elements may be used. The nucleic acid modification may render the nucleic acid more stable and/or less susceptible to degradation under certain conditions. For example, in some instances, the nucleic acids are nuclease-resistant.

Methods of synthesizing nucleic acids (*e.g.*, ssDNA or dsDNA, or ssRNA or dsRNA) are known in the art and are described, for example, in U.S. Patent Nos. 5,143,854 and 5,445,934, herein incorporated in their entirety.

Nucleic acids may be synthesized *in vitro*. Methods for synthesizing nucleic acids, including automated nucleic acid synthesis, are also known in the art. Nucleic acids having modified backbones, such as backbones comprising phosphorothioate linkages, and including those comprising chimeric modified backbones may be synthesized using automated techniques

employing either phosphoramidate or H-phosphonate chemistries. (F. E. Eckstein, "Oligonucleotides and Analogues - A Practical Approach" IRL Press, Oxford, UK, 1991, and M. D. Matteucci and M. H. Caruthers, *Tetrahedron Lett.* 21, 719 (1980)) Aryl- and alkyl-phosphonate linkages can be made, *e.g.*, as described in U.S. Patent No. 4,469,863; and alkylphosphotriester linkages (in which the charged oxygen moiety is alkylated), *e.g.*, as described in U.S. Patent No. 5,023,243 and European Patent No. 092,574, can be prepared by automated solid phase synthesis using commercially available reagents. Methods for making other DNA backbone modifications and substitutions have been described. Uhlmann E et al. (1990) *Chem Rev* 90:544; Goodchild J (1990) *Bioconjugate Chem* 1:165; Crooke ST et al. (1996) *Annu Rev Pharmacol Toxicol* 36:107-129; and Hunziker J et al. (1995) *Mod Synth Methods* 7:331-417.

Nucleic acids may additionally or alternatively comprise modifications in their sugars. For example, a β -ribose unit or a β -D-2'-deoxyribose unit can be replaced by a modified sugar unit, wherein the modified sugar unit is for example selected from β -D-ribose, α -D-2'-deoxyribose, L-2'-deoxyribose, 2'-F-2'-deoxyribose, arabinose, 2'-F-arabinose, 2'-O-(C₁-C₆)alkyl-ribose, preferably 2'-O-(C₁-C₆)alkyl-ribose is 2'-O-methylribose, 2'-O-(C₂-C₆)alkenyl-ribose, 2'-[O-(C₁-C₆)alkyl-O-(C₁-C₆)alkyl]-ribose, 2'-NH₂-2'-deoxyribose, β -D-xylo-furanose, α -arabinofuranose, 2,4-dideoxy- β -D-erythro-hexo-pyranose, and carbocyclic (described, for example, in Froehler J (1992) *Am Chem Soc* 114:8320) and/or open-chain sugar analogs (described, for example, in Vandendriessche et al. (1993) *Tetrahedron* 49:7223) and/or bicyclosugar analogs (described, for example, in Tarkov M et al. (1993) *Helv Chim Acta* 76:481).

Nucleic acids may comprise modifications in their bases. Modified bases include modified cytosines (such as 5-substituted cytosines (*e.g.*, 5-methyl-cytosine, 5-fluoro-cytosine, 5-chloro-cytosine, 5-bromo-cytosine, 5-iodo-cytosine, 5-hydroxy-cytosine, 5-hydroxymethyl-cytosine, 5-difluoromethyl-cytosine, and unsubstituted or substituted 5-alkynyl-cytosine), 6-substituted cytosines, N₄-substituted cytosines (*e.g.*, N₄-ethyl-cytosine), 5-aza-cytosine, 2-mercapto-cytosine, isocytosine, pseudo-isocytosine, cytosine analogs with condensed ring systems (*e.g.*, N,N'-propylene cytosine or phenoxazine), and uracil and its derivatives (*e.g.*, 5-fluoro-uracil, 5-bromo-uracil, 5-bromovinyl-uracil, 4-thio-uracil, 5-hydroxy-uracil, 5-propynyl-uracil), modified guanines such as 7-deazaguanine, 7-deaza-7-substituted guanine (such as 7-deaza-7-(C₂-C₆)alkynylguanine), 7-deaza-8-substituted guanine, hypoxanthine, N₂-substituted guanines (*e.g.* N₂-methyl-guanine), 5-amino-3-methyl-3H,6H-thiazolo[4,5-d]pyrimidine-2,7-dione, 2,6-diaminopurine, 2-aminopurine, purine, indole, adenine, substituted adenines (*e.g.* N₆-

methyl-adenine, 8-oxo-adenine) 8-substituted guanine (*e.g.* 8-hydroxyguanine and 8-bromoguanine), and 6-thioguanine. The nucleic acids may comprise universal bases (*e.g.* 3-nitropyrrole, P-base, 4-methyl-indole, 5-nitro-indole, and K-base) and/or aromatic ring systems (*e.g.* fluorobenzene, difluorobenzene, benzimidazole or dichloro-benzimidazole, 1-methyl-1H-[1,2,4]triazole-3-carboxylic acid amide). A particular base pair that may be incorporated into the oligonucleotides of the invention is a dZ and dP non-standard nucleobase pair reported by Yang et al. NAR, 2006, 34(21):6095-6101. dZ, the pyrimidine analog, is 6-amino-5-nitro-3-(1'-β-D-2'-deoxyribofuranosyl)-2(1H)-pyridone, and its Watson-Crick complement dP, the purine analog, is 2-amino-8-(1'-β-D-1'-deoxyribofuranosyl)-imidazo[1,2-a]-1,3,5-triazin-4(8H)-one.

10 In exemplary embodiments, nucleic acid nanostructures comprise single-stranded genomic DNA. For example, nucleic acid nanostructures may comprise linear or circular single-stranded M13 plasmid DNA. In some embodiments, nucleic acid nanostructures do not comprise plasmid DNA.

It should be appreciated that nucleic acid nanostructures of the present disclosure, in some embodiments, do not include condensed nucleic acid. As used herein, “condensed nucleic acid” refers to compacted nucleic acid, for example, that is twisted and coiled upon itself (*see, e.g.,* Teif VB, et al. *Progress in Biophysics and Molecular Biology* 105 (3): 208–222, incorporated by reference herein). The term “condensed nucleic acid” excludes nucleic acid nanostructures that have a distinct 2D or 3D architecture.

20 It should also be appreciated that nucleic acid nanostructures of the present disclosure, in some embodiments, do not include coding nucleic acid. That is, in some embodiments, nucleic acid nanostructures comprise non-coding nucleic acids (*e.g.,* nucleic acids that do not encode proteins). As used herein, a “coding nucleic acid” refers to a nucleic acid containing a nucleotide sequence that specifies a sequence of amino acids of a protein (*e.g.,* a therapeutic protein). Thus, a “non-coding nucleic acid” is a nucleic acid that does not specify a sequence of amino acids of a protein and, accordingly, is not transcribed into RNA or translated into protein. In other embodiments, it should be understood that a nucleic acid nanostructure may contain one or more coding nucleic acids.

In some embodiments, nucleic acids used to make nucleic acid nanostructures do not code for any amino acid. In some embodiments, nucleic acids used to make nucleic acid nanostructures do not code for more than 1, 2, 3, 4 or 5 consecutive amino acids.

In some embodiments, nucleic acids used to make nucleic acid nanostructures do not include art-recognized regulatory elements/sequences such as promoters, enhancers, polyA sequences and/or ribosomal binding site sequences.

In some embodiments, nucleic acids used to make nucleic acid nanostructures are not plasmids.

In some embodiments, nucleic acids used to make nucleic acid nanostructures contain more than one nucleic acid, and the nucleic acids are different from each other. That is, the
5 nucleic acids of a nucleic acid nanostructure may comprise a plurality of different nucleic acids.

In some embodiments, nucleic acid nanostructures are not encapsulated by or coated with (*e.g.*, linked to) lipids. For example, a variety of gene delivery methods of the prior art make use of nucleic acid nanostructures that are linked to hydrophobic moieties and/or covered by lipids (*e.g.*, such as a lipid bilayer), which function to prevent nuclease degradation (*see, e.g.*, WO
10 2013148186 A1). The present disclosure, in some embodiments, excludes nucleic acid nanostructures that are linked to hydrophobic moieties and/or covered by lipids. In other embodiments, however, a nucleic acid nanostructure may contain one or more nucleic acids linked to one or more hydrophobic moieties and/or lipids.

Nucleic acid nanostructures of the present disclosure have a variety of *in vitro* and *in vivo*
15 uses. In some embodiments, may be used as scaffolds, cages or multifunctional carriers for delivering an antigen that is intended for use *in vivo* and/or *in vitro*. A nucleic acid nanostructure may be delivered by any suitable delivery method, for example, intravenously or orally.

The present disclosure contemplates imparting addressability to nucleic acid nanostructures. For example, nucleic acid nanostructures may be modified by site-specific
20 attachment of targeting moieties such as proteins, ligands or other small biomolecules. In some embodiments, nucleic acid nanostructures may comprise nucleic acid “staple” strands, as described above, that serve as handles for nanometer-specific placement of accessory molecules (*e.g.*, biotin/streptavidin) at virtually any position on or within the structure (*see, e.g.*, Stein et al. *Chemphyschem.* 12(3), 689–695 (2011); Steinhauer et al. *Angew Chem. Int. Ed. Engl.* 48(47),
25 8870–8873 (2009); Stein et al. *J. Am. Chem. Soc.* 133(12), 4193–4195 (2011); Kuzyk et al. *Nature* 483(7389), 311–314 (2012); and Ding et al. *J. Am. Chem. Soc.* 132(10), 3248–3249 (2010); Yan et al. *Science* 301(5641), 1882–1884 (2003); and Kuzuya et al. *Chembiochem.* 10(11), 1811–1815 (2009), each of which is incorporated by reference herein).

In some embodiments, nucleic acids of nanostructures provided herein may be modified
30 (*e.g.*, covalently modified) with a linker (*e.g.*, biotin linker) during synthesis or via enzymatic means (*see, e.g.*, Jahn et al. *Bioconjug. Chem.* 22(4), 819–823 (2011) incorporated by reference herein). Such methods may also be used to position reaction systems on nucleic acid nanostructures through the chemical biotinylation of enzyme molecules (*see, e.g.*, Voigt et al. *Nat. Nanotechnol.* 5(3), 200–203 (2010)).

A more generalized antibody-based binding approach may also be used to link target proteins to nucleic acid nanostructures at defined distances (*see, e.g.*, Williams et al. *Angew Chem. Int. Ed. Engl.* 46(17), 3051–3054 (2007); and He Y et al. *J. Am. Chem. Soc.* 128(39), 12664–12665 (2006), each of which is incorporated by reference herein). Thus, in some
5 embodiments, nucleic acid nanostructures may be linked to one or more antibodies.

In other embodiments, DNA aptamers, which adopt a specific secondary structure with high binding affinity for a particular molecular target, may be used as linkers, thereby eliminating the need for protein linkers (*see, e.g.*, Ellington et al. *Nature* 346(6287), 818–822 (1990); Chhabra et al. *J. Am. Chem. Soc.* 129(34), 10304–10305 (2007); and Rinker et al. *Nat.*
10 *Nanotechnol.* 3(7), 418–422 (2008), each of which is incorporated by reference herein).

The present disclosure also contemplates the use of recombinant genetic engineering methods to selectively add affinity tags or other peptide linkers to nucleic acid nanostructures. For example, polyhistidine sequence consisting of multiple histidine residues on the C- or N-terminus end of a target protein is a commonly used tag for affinity-based purification. This, in
15 turn, can be linked via nickel-mediated interaction to a nitrilotriacetic acid molecule that is covalently conjugated to an amine (*see, e.g.*, Goodman et al. *Chembiochem.* 10(9), 1551–1557 (2009), incorporated by reference herein) or thiol-modified (*see, e.g.*, Shen et al. *J. Am. Chem. Soc.* 131(19), 6660–6661 (2009), incorporated by reference herein) nucleic acid. Through this method, fluorescent proteins may be positioned both periodically and specifically on nucleic acid
20 nanostructures (Goodman et al. (2009); and Shen et al. (2009)). Similarly, SNAP and HaloTag® peptide sequences, also used for affinity purification of recombinant proteins, may be utilized for the orthogonal decoration of nucleic acid nanostructures with different protein or enzyme species (*see, e.g.*, Sacca et al. *Angew Chem. Int. Ed. Engl.* 49(49), 9378–9383 (2010), incorporated by reference herein). A related approach involving the creation of chimeric proteins conjugated to a
25 DNA-binding domain, can eliminate the often complex chemical synthesis techniques and toxic compounds (*e.g.*, nickel) necessary to stably conjugate affinity tag binding partners to oligonucleotide strands. Further, zinc-finger domains that recognize specific double-stranded sequences may be used to arrange fluorescent proteins at specific locations on nucleic acid nanostructures of the present disclosure (*see, e.g.*, Nakata et al. *Angew Chem. Int. Ed. Engl.*
30 51(10), 2421–2424 (2012), incorporated by reference herein).

An adjuvant (*e.g.*, CpG) and/or antigen may be covalently or non-covalently attached to a nucleic acid nanostructure. The location and nature of the linkage between the adjuvant (*e.g.*, CpG) and/or antigen and the nucleic acid nanostructure will depend upon the function of the adjuvant (*e.g.*, CpG) and/or antigen. As an example, an adjuvant (*e.g.*, CpG) and/or antigen may
35 be intended to release (including slow release) from the nanostructure, and in that case, the

linkage between the adjuvant (e.g., CpG) and/or antigen and the nanostructure may be chosen to achieve the desired release profile. In some embodiments, an adjuvant (e.g., CpG) and/or antigen may be inactive in its bound form and activated only when released.

5 In some embodiments, an adjuvant (e.g., CpG) and/or antigen may be combined with nucleic acids during assembly (e.g., self-assembly) of nanostructures, or an adjuvant (e.g., CpG) and/or antigen may be combined with pre-formed nucleic acid nanostructures.

10 Adjuvant (e.g., CpG) and/or antigen may be linked to an interior surface (in the interior compartment) or an exterior surface of a nanostructure. Adjuvant (e.g., CpG) and/or antigen may be arranged in various configurations. Upon hybridization of handles to anti-handles, adjuvant (e.g., CpG) and/or antigen become indirectly linked to nucleic acid nanostructures. It should be understood that nanostructures of the present disclosure permit precise placement of an adjuvant (e.g., CpG) and/or antigen or more than one adjuvant (e.g., CpG) and/or antigen (e.g., a combination of different adjuvant (e.g., CpG) and/or antigen) on the interior and/or exterior surface of the nanostructures.

15 Nucleic acid nanostructures of the present disclosure permit high-density “packing” of adjuvant (e.g., CpG) and/or antigen on and into the nanostructures. In some embodiments, a nucleic acid nanostructures is decorated with one adjuvant (e.g., CpG) and/or antigen per 50 nm² to 75 nm². In some embodiments, a nucleic acid nanostructure is decorated with one adjuvant (e.g., CpG) and/or antigen per 50 nm², 55 nm², 60 nm², 65 nm², 70 nm² or 75 nm². For example, 20 using a rhombic-lattice spacing for a 30 nm tall, 60 nm diameter cylindrical nanostructure, 72 positions on the exterior of the nanostructure and 84 positions on the interior may be occupied by adjuvant (e.g., CpG) and/or antigen. For larger nanostructures, for example, those with two 30 nm x 60 nm cylindrical nanostructures, the number of positions occupied by adjuvant (e.g., CpG) and/or antigen is doubled. For even larger nanostructures, for example, those with three 30 nm x 25 60 nm cylindrical nanostructures, the number of positions occupied by adjuvant (e.g., CpG) and/or antigen tripled, and so on.

The present disclosure contemplates, in some aspects, the delivery of nucleic acid nanostructures, or nucleic acid nanostructures loaded with an adjuvant (e.g., CpG) and/or antigen, systemically or to localized regions, tissues or cells. Any adjuvant (e.g., CpG) and/or 30 antigen gent may be delivered using the methods of the present disclosure provided that it can be loaded onto or into the nucleic acid nanostructure. Because such processes are relatively innocuous, it is expected that virtually any adjuvant (e.g., CpG) and/or antigen may be used.

The length of a CpG adjuvant may vary. For example, the length may be 10-100 nucleotides (nt), 10-50 nt, or 10-20 nt.

Adjuvants

An “adjuvant” is an agent that enhances an immune response to an antigen. In some embodiments, an adjuvant is a CpG oligonucleotide. CpG oligonucleotides are short single-stranded synthetic DNA molecules that contain a cytosine triphosphate deoxynucleotide (“C”) followed by a guanine triphosphate deoxynucleotide (“G”). The “p” refers to the phosphodiester, or modified phosphorothioate (PS), linkage between consecutive nucleotides. CpG oligonucleotides typically enhance the immunostimulatory effect of nucleic acid nanostructures (Li, J. et al. ACS NANO, 5(11): 8783-8789, 2011; Schuller, V. et al. ACS NANO, 5(12): 9696-9702, 2011). For example, after they are taken up by cells, CpG oligonucleotides, which are a hallmark of microbial DNA, are recognized by the endosomal Toll-like receptor 9 (TLR9) that activates downstream pathways to induce immunostimulatory effects, producing high-level secretion of various pro-inflammatory cytokines including tumor necrosis factor (TNF)- α , interleukin (IL)-6, and IL-12. In some embodiments, CpG oligonucleotides are linked to an interior surface of a nucleic acid nanostructure. In some embodiments, CpG oligonucleotides are linked to an exterior surface of a nucleic acid nanostructure. In some embodiments, a nucleic acid nanostructure has CpG oligonucleotides linked to both an interior and exterior surface. Other examples of adjuvants include, without limitation, lipopolysaccharide and polyI:C (dsRNA mimic).

A “subject” to which administration is contemplated includes, but is not limited to, humans (*e.g.*, a male or female of any age group, *e.g.*, a pediatric subject (*e.g.*, infant, child, adolescent) or adult subject (*e.g.*, young adult, middle-aged adult or senior adult)) and/or other non-human animals, for example mammals (*e.g.*, primates (*e.g.*, cynomolgus monkeys, rhesus monkeys), including commercially relevant mammals such as cattle, pigs, horses, sheep, goats, cats, and/or dogs), birds (*e.g.*, commercially relevant birds such as chickens, ducks, geese, and/or turkeys), reptiles, amphibians, and fish. In some embodiments, the non-human animal is a mammal. The non-human animal may be a male or female and at any stage of development. A non-human animal may be a transgenic animal.

Nucleic acid nanostructures and compositions containing nucleic acid nanostructures may be administered to a subject (*e.g.*, a human or non-human subject) subcutaneously or intravenously (*e.g.*, single/multiple injection(s) or continuous infusion), or by other means.

In some embodiments, nucleic acid nanostructures are administered to a subject as a component of a polymeric gel composition. The polymeric gel composition may be biocompatible and/or biodegradable. In some embodiments, the polymeric gel composition is formed from, and/or comprises at least one polylactic acid, polyglycolic acid, PLGA polymers, alginates and alginate derivatives, gelatin, collagen, agarose, natural and synthetic

polysaccharides, polyamino acids such as polypeptides particularly poly(lysine), polyesters such as polyhydroxybutyrate and poly-epsilon-caprolactone, polyanhydrides; polyphosphazines, poly(vinyl alcohols), poly(alkylene oxides) particularly poly(ethylene oxides), poly(allylamines)(PAM), poly(acrylates), modified styrene polymers such as poly(4-aminomethylstyrene), pluronic polyols, polyoxamers, poly(uronic acids), poly(vinylpyrrolidone) and copolymers of the above, including graft copolymers (*see, e.g.*, International Publication No. WO2009102465).

In some embodiments, the present disclosure provides methods for manipulating, directly in the body, dendritic-cell recruitment and activation. Immature dendritic cells patrol peripheral tissues, and on uptake of foreign substances (*e.g.*, antigen), they may mature to express on their surface molecules (*e.g.*, the receptor CCR7 and major histocompatibility complex (MHC) antigen) to facilitate lymph-node homing and subsequent antigen presentation to T-cells, respectively. Elements of infection that mobilize and activate dendritic cells include inflammatory cytokines, and “danger signals” related specifically to the infectious agent. Cytosine-guanosine oligonucleotide (CpG-ODN) sequences are uniquely expressed in bacterial DNA, and are potent danger signals that stimulate mammalian dendritic-cell activation and dendritic-cell trafficking. Thus, in some embodiments, the present disclosure provides methods for administering to a subject nucleic acid nanostructures that comprise antigen (*e.g.*, cancer antigen) and danger signals (*e.g.*, CpG oligonucleotides).

Antigens

An “antigen”, as used herein, may refer to any biomolecule that may induce an immune response. In some embodiments, an antigen is a peptide, a protein or polypeptide, or a nucleic acid. In some embodiments, an antigen is a cancer antigen. A cancer antigen may be a component or element of a cancer cell or a biomolecule isolated from a cancer cell (*e.g.*, a biomolecule known to be associated with cancerous tumors). In some embodiments, a cancer antigen comprises a biomolecule (*e.g.*, a peptide or polypeptide) that is overexpressed or overactivated in cancer cells, relative to normal and non-cancerous cells.

Non-limiting examples of cancer antigens include Her2 peptides (for vaccination against selected breast cancers); NY-ESO-1 peptides (for vaccination against selected bladder cancers); HPV16 E7 peptides (for vaccination against selected cervical cancers); carcinoembryonic antigen (for vaccination against selected colorectal cancers); Wilms’ tumor 1 (WT1) peptides (for vaccination against selected leukemias); MART-1, gp100, and tyrosinase (for vaccination against selected melanomas); URLC10, VEGFR1, and VEGFR2 (for vaccination against selected non-small lung cell cancers); survivin (for vaccination against selected ovarian cancers);

MUC1 (for vaccination against selected pancreatic cancers); MUC2 (for vaccination against selected prostate cancers); telomerase (TERT); Indoleamine 2,3-dioxygenase (IDO1); CTAG1B, and VEGF receptors (FLT1 and KDR). In some embodiments, a cancer antigen is as described in Tagliamonte, M. et al. "Antigen-specific vaccines for cancer treatment", *Hum Vaccin Immunother.* 2014 Nov; 10(11): 3332–3346.; or Pol, J. et al. "Trial Watch: Peptide-based anticancer vaccines", *Oncoimmunology.* 2015 Apr; 4(4): e974411.

In some embodiments, a cancer antigen is selected from the following: CEA; gp100; Pmel17; mammaglobin-A; Melan-A; MART- 1 ; NY-BR-1; ERBB2; OA1; PAP; PSA; RAB38; NY-MEL- 1; TRP-1; gp75; TRP-2; tyrosinase; WT1; CD33; BAGE-1; D393-CD20n; Cyclin-A1; GAGE-1,2,8; GAGE-3,4,5,6,7; GnTVf; HERV- K-MEL; KK-LC-1; KM-HN-1; LAGE-1; LY6K; MAGE-A1; MAGE-A2; MAGE- A3; MAGE-A4; MAGE-A6; MAGE-A9; MAGE-A10; MAGE-A12m; MAGE-C1; MAGE-C2; mucink; NA88-A; NY-ESO-1; LAGE-2; SAGE; Spl7; SSX-2; SSX-4; survivin; BIRC5; TAG- 1 ; TAG-2; TRAG-3; TRP2-INT2g; XAGE-1b; GAGED2a; BCR-ABL (b3a2); adipophilin; AIM-2; ALDH1A1; BCLX(L); BING-4; CALCA; CD45; CD274; CPSF; cyclin D1; DKK1; ENAH (hMena); EpCAM; EphA3; EZH2; FGF5; glypican-3; G250; MN; CAIX; HER-2; neu; HLA-DOB; Hepsin; IDO1; IGF2B3; IL13Ralpha2; Intestinal carboxyl esterase; alpha-foetoprotein; Kallikrein 4; KIF20A; Lengsin; M-CSF; MCSP; mdm-2; Meloe; Midkine; MMP-2; MMP-7; MUC1; MUC5AC; p53; PAX5; PBF; PRAME; PSMA; RAGE- 1; RGS5; RhoC; RNF43; RU2AS; secernin 1; SOX10; STEAP1; Telomerase; TPBG; and VEGF.

Methods of Use

The nucleic acid nanostructures described herein (e.g., comprising antigen, CpG ligand, and/or oligolysine-PEG) may be used vaccines to induce an immune response to a particular antigen, such as a tumor antigen or a microbial (e.g., bacterial or viral) antigen.

In some embodiments, administration of the nanostructure results in an at least 2-fold or at least 3-fold reduction in tumor volume.

In some embodiments, administration of the nanostructure stimulates cytokine production in dendritic cells of the subject, wherein the cytokine production is at least 10%, at least 15%, or at least 20% higher than cytokine production by dendritic cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

In some embodiments, administration of the nanostructure stimulates Interleukin-10 (IL10) production in dendritic cells of the subject. In some embodiments, administration of the nanostructure stimulates Interleukin-12 (IL12) production in dendritic cells of the subject.

In some embodiments, administration of the nanostructure increases antigen uptake in dendritic cells of the subject, wherein the antigen uptake is at least 10%, at least 15%, or at least 20% higher than antigen uptake by dendritic cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

5 In some embodiments, administration of the nanostructure stimulates a stronger Th1 immune response, relative to stimulation of a Th2 response. The Th1 response stimulated may be at least 10%, at least 15%, at least 20%, at least 25%, at least 30%, at least 35%, at least 40%, at least 45%, or at least 50% stronger than a Th2 response stimulated by administration of the nanostructure.

10 In some embodiments, the Th1 immune response is characterized by expression of CD69 and CD8 on T cells. In some embodiments, the expression of CD69 and/or CD8 on T cells of a subject following administration of the nanostructure may be at least 10%, at least 15%, at least 20%, at least 25%, at least 30%, at least 35%, at least 40%, at least 45%, or at least 50% higher than expression of the same molecule in T cells of a subject administered a control (e.g., antigen
15 only or antigen and free CpG oligonucleotides).

In some embodiments, administration of the nanostructure stimulates CD8+ T cell proliferation by at least 10%, at least 15%, or at least 20% relative to CD8+ T cell proliferation in control cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

In some embodiments, administration of the nanostructure stimulates IFN- γ expression in
20 OT-I CD8+ T cells of the subject, wherein the IFN- γ expression is at least 10%, at least 15%, or at least 20% higher than IFN- γ expression by in OT-I CD8+ T cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

Additional Embodiments

25 The present disclosure provides the following additional embodiments:

1. A nucleic acid nanostructure comprising a plurality of uniformly spaced CpG ligands and a plurality of antigens, wherein the nucleic acid nanostructure is coated and covalently crosslinked with oligolysine-polyethylene glycol (PEG) copolymer, optionally at a N:P (nitrogen in lysine to phosphorus in nucleic acid) ratio of 0.1:1 to 1:1.
- 30 2. The nucleic acid nanostructure of paragraph 1, wherein each CpG ligand of the plurality of CpG ligands is uniformly spaced 2 nm – 10 nm (e.g., 2.5 nm, 3.5 nm, 5 nm or 7 nm) from any other CpG ligand, optionally wherein the nucleic acid nanostructure comprises 10-100 (e.g., 10-50 or 10-20) CpG ligands.

3. The nucleic acid nanostructure of paragraph 1, wherein each CpG ligand of the plurality of CpG ligands is uniformly spaced 3 nm-5 nm, 3 nm-4 nm, or 3.5 nm from any other CpG ligand.
4. A nucleic acid nanostructure comprising a plurality of CpG ligands and a plurality of
5 antigens, wherein each CpG ligand of the plurality of CpG ligands is uniformly spaced 3 nm-5 nm, 3 nm-4 nm, or 3.5 nm from any other CpG ligand.
5. The nucleic acid nanostructure of paragraph 4, wherein the nucleic acid nanostructure is coated and covalently crosslinked with oligolysine-polyethylene glycol (PEG) copolymer.
6. The nucleic acid nanostructure of any one of paragraphs 1-5, wherein the nucleic acid
10 nanostructure is a DNA origami nanostructure.
7. The nucleic acid nanostructure of paragraph 6, wherein the DNA origami nanostructure is a 126-helix DNA origami nanostructure.
8. The nucleic acid nanostructure of any one of paragraphs 1-7, wherein the plurality of antigens comprise ovalbumin.
9. The nucleic acid nanostructure of any one of paragraphs 1-8, wherein the plurality of
15 antigens are covalently linked to the nanostructure.
10. The nucleic acid nanostructure of paragraph 9, wherein the plurality of antigens are covalently linked to free amine groups of the nucleic acid nanostructure.
11. A method of inducing a Th1 polarized immune response in cells, the method comprising
20 administering to a subject the nucleic acid nanostructure of any one of paragraphs 1-10.
12. A method of inducing a Th1 polarized immune response in cells, the method comprising administering to a subject a nucleic acid nanostructure comprising a plurality of uniformly spaced CpG ligands and a plurality of antigens.
13. The method of paragraph 11 or 12 wherein the subject has a tumor (e.g., a cancerous
25 tumor).
14. The method of paragraph 13, wherein the volume of the tumor is reduced at least 2-fold relative to control.
15. The method of paragraph 14, wherein the volume of the tumor is reduced at least 3-fold relative to control.
16. The method of any one of paragraphs 11-15, wherein the nucleic acid nanostructure is
30 administered to the subject multiple times (e.g., at least 2 times, at least 3 times, etc.).

EXAMPLES

Example 1. Fabrication of square-lattice blocks (SQBs) with different CpG spacing

Using scaffold p8634 as template, the folding of SQBs with square-lattice blocks (comprising 126 helices) were designed using Cadnano software. One end of the helices was flat, while the other end of the helices had some extruding extra scaffold. See FIGS. 2A-2D. FIG. 2A includes representative images showing the 3D nanostructure of the SQBs. FIG. 2B shows representative TEM images of SQB nanostructures folded at a 80-5040-18 temperature ramp. Eight (8) Cy5 fluorophores were appended to the extruding side through anti-handle strategy (FIG. 2C). Multi sides and size of the SQB DNA origami corresponding to the Cadnano 3D cartoon are depicted in the TEM images in FIG. 2D. The following four spacing strategies were designed, wherein two of the adjacent CpG sequences have a distance of 2.5 nm (CpG1), 3.5 nm (CpG2), 5 nm (CpG3) and 7 nm (CpG4) on the flat face of the helices, and 18 CpG sequences were applied (FIG. 2E).

Example 2. Different CpG-Cy5-SQBs showed concentration-dependent cellular uptake by 293 T cells and mouse bone marrow dendritic cells (BMDCs)

For cell uptake studies, polyethylene glycol (PEG) purification was first used to purify all the DNA origami nanostructures of Example 1 from extra staple strands (FIGs. 3A, 3B). The CpG0 DNA origami structures (no CpG ligand) were then coated with oligolysine-PEG (K10PEG5) and cultured in 10% fetal bovine serum (FBS) containing medium. the K10PEG5 stabilized the CpG0 DNA origami structures and protected them from denaturation induced by physiological salt concentrations and degradation mediated by nucleases (FIG. 3C). Three time points were assessed: culturing for 18 hours (h), 48 h, and 72 h. 293T cells and mouse bone marrow dendritic cells (BMDCs) were then transfected with 1 nm CpG-Cy5-SQBs (FIG. 3D). Dark coloration in the figures demonstrates presence of CpG-Cy5-SQBs. Flow cytometry data confirmed cell uptake by BMDCs when applying different concentration of CpG-Cy5-SQBs (FIGs. 3E, 3F). Thus, the K10PEG5-coated CpG-DNA nanostructures retained stability in the FBS-containing media and could be taken up by 293T cells and mouse BMDCs successfully.

Example 3. Dendritic cell maturation and Th1 immune response polarization

Five (5) CpG-Cy5-SQBs were co-cultured with immature mouse BMDCs. Free CpG-ODN (200 nM P8634) was used as a positive control. It was found that BMDCs underwent severe apoptosis in the CpG-ODN control group compared to CpG-Cy5-SQB groups (FIGs. 4A, 4B).

Interestingly, higher concentrations of CpG-Cy5-SQBs showed decreased cell apoptosis and cell death (FIG. 4B). Staining for DC maturation markers CD40 (FIG. 4C), CD80 (FIG. 4D), CD86

(FIG. 4E), MHC II (FIG. 4F) revealed that the CpG2 and CpG3 at spacing of 3.5 nm and 5 nm could greatly increase DC maturation signaling compared to CpG0. Through ELISA, it was found that CpG0 barely stimulates expression of IL-12 and IL-10 (indication of low immunogenicity of the origami), however, CpG2 could stimulate DCs to generate more IL-12 but less IL-10 (FIG. 4H). These results therefore suggest that CpG2 (spacing at 3.5 nm) favorably stimulate Th1 polarized immune responses which may greatly stimulate downstream Th1 CD4 cell and CD8 T cell activation.

Example 4. Antigen uptake and presentation

10 The model antigen OVA was conjugated to DNA origami as proof-of-concept for vaccine fabrication (FIG. 5A). OVA protein was observed on the extruding side of the SQBs by TEM image (FIG. 5B). By co-culturing with BMDCs, it was found that conjugated CpG-OVA greatly increased antigen uptake by BMDCs compared to same amount of free OVA with CpG-Cy5-SQBs or free CpG ODN (FIG. 5C). DEC-205 is reported be a marker of activated DCs
15 involved in protein uptake. DEC205 was greatly increased in all the DNA origami groups when the antigen is co-delivered, especially in the CpG2 group, which likely contributes to increased antigen-uptake (FIG. 5D). Double positive population of CD86 and MHC DCs was significantly increased in CpG2 group (FIG. 5E). Similar results applied when single positive population was plotted. The presentation of OVA peptide SIINFEKL, an epitope presented by the mouse class I
20 major histocompatibility, was significantly increased in all the origami vaccine applied groups, with CpG2 outperformed than all other versions (FIG. 5F). These data suggested that co-delivery of antigen and adjuvant is important for DC cell activation, and SQB nanoparticle might play an important role in MHC I cross-presentation pathway.

25 Example 5. DNA origami stabilize Tregs in the splenocyte while stimulating CD69 expression on CD8 T cells

Splenocytes were collected from C57BL/6 mouse and stimulated with different CpG-Cy5-SQBs. Naïve T cell early activation through cytokines secreted by DCs was observed. CD3+ T cells did not uptake the DNA origami structures (data not shown). Instead, Cy5 signal
30 mostly existed in CD3- cells that might be DCs or macrophages. After two-day stimulation, it was found that CpG-Cy5-SQBs would not apparently increase suppressive FoxP3+CD25+CD4+ Tregs compared to CpG-OND (FIGs. 6A, 6B). However, all the CpG-Cy5-SQBs could stimulate early activation marker CD69 expression on CD8+ and CD4+ T cells (FIGs. 6C, 6D). CpG2 groups showed enhanced expression of CD69+CD8+ T cells compared to CpG0. However,
35 CpG-ODN could strongly stimulate expression of CD69+CD4+ T cells compared to CpG-Cy5-

SQB (FIGs. 6E, 6F) (N=7). CD69 is an early activation marker, involved in lymphocyte proliferation and also contributing to the differentiation of Treg cells. These results suggested that CpG-Cy5-SQB might favorably stimulate Th1 immune response, which is indicated by CD8 early activation and un-upregulated Tregs, whereas CpG-ODN might stimulate a Th2 preferable response by upregulating Tregs, which is less appreciated in cancer immunotherapy.

Example 6. OT-I and OT-II T cell stimulation *in vitro* and tumor cell killing *in vitro*.

DNA origami vaccine pulsed DCs were cocultured with OT-I CD8+ T cells and OT-II CD4+ T cells. The results showed that CD8+ T cell proliferation was significantly increased in CpG2 (3.5nm spacing) pulsed DC coculture group (FIGs. 7A, 7B). IFN- γ and that IL-2 expression on OT-I CD8+ T cells was strikingly increased in conjugated CpG-OVA-SQB groups (FIGs. 7C, 7D), while the unconjugated counterpart only showed limited secretions. Especially CpG2 behaved better than other CpG spacings, indicating improved cross-presentation and CD8 proliferation. The results also showed that IFN- γ expression in OT-II CD4+ T cells was significantly increased in CpG2 group where antigen is co-delivered (FIG. 7C). In a tumor cell killing study, delivery of CpG2 (spacing at 3.5 nm) led to significant cell killing by activated CD8+ T cells (FIGs. 7F, 7G). These data suggest that: (1) co-presentation of antigen and adjuvant is important for effective DC stimulation, and DNA origami provides a superior platform for co-delivery that could improve antigen presentation by DCs and downstream Th1 polarization; and (2) antigen and adjuvant presentation together through DNA origami vaccine might preferentially increase MHC-I peptide presentation to OT-I T cells and increase CD8+ T cells proliferation and function.

Example 7. Control spacing for CpG2.

To verify if a minimal CpG dimer-trigger unit spacing at 3.5nm is important for TLR9 dimerization and activation, CpG2-dt were designed with 9 pairs of dimer-trigger units spaced out. Irregular spacing CpGi was also designed as positive control (FIG. 8A). The proliferation of CFSE positive OT-I CD8 T cells cocultured with pulsed DCs demonstrated that CpG2-dt seems to have similar stimulation effect compared to CpG2 (FIG. 8B). However, CpGi interrupted this effect. In the tumor cell-killing study, CpG2-dt showed similar results to CpG2, although CpG2 still showed the best tumor killing effects (FIG. 8C, D).

Example 8. Therapeutic and prophylactic effects in mouse melanoma tumor model.

An aggressive melanoma mouse model was set up using 0.5 million B16-OVA cells. Three treatments of CpG2-OVA-SQB vaccine were administered subcutaneously (FIG. 9A).

Tumor growth was greatly inhibited compared to control free CpG + free OVA + free SQB applied groups and other spacing vaccines (FIGs. 9B, 9C). Note that the CpG and OVA administered were low doses compared to prior studies in the literature. In some mice, minimal tumor growth was noted as long as the treatment was given (FIG. 9B). Additionally, overall survival was greatly improved in the CpG2 vaccine applied group (FIG. 9D). In a prophylactic study, two doses of CpG2-OVA-SQBs were injected subcutaneously on day 1 and day 7, and then inoculated the mice with tumor cells (FIG. 9E). On day 28, measurable tumors were observed in control groups and in 40% of the free CpG and free OVA applied group (FIG. 9F). No tumors were observed in DNA origami vaccine treated group. All 5 mice in the control group had died by the conclusion of the study. 60% of mice in the free CpG and free OVA applied group had died. Only one mouse in CpG2-OVA-SQBs applied group was dead at the end point of the study (FIG. 9G). These results verified the effectiveness of the DNA origami vaccine in a murine melanoma model.

15 **Example 9. Immune cell profiling in animals post vaccination.**

After the tumor mice were given three treatments of vaccine, the mice were sacrificed, and the lymph nodes and tumor tissues were processed to single cell suspension for flow cytometry. In the lymph node, more CD11c+ DC cells were found in the CpG2 group (FIGs. 10A, 10C). There were also more CD11c+ in group of CpG an OVA delivered separately on SQB (FIG. 10C), however, this did not correlated to DC and T cell activation which proved the importance of co-delivery. Treg cells were proved high *in vivo* again when free CpG and free OVA were applied (FIGs. 10B, 10D). MHC II and CD40 double positive mature DCs significantly increased in CpG2 group (FIG. 10E). SIINFEKL MHCI + expression was remarkably increased in CpG2 compared to other spacing strategy (FIG. 10F). CD8 and CD4 T cells were activated the most in CpG2 group indicated by CD69 expression and memory marker CD44 (FIGs. 10G, 10H). CD8 OVA tetramer cells increased about 7 times in the lymph node in CpG2 group (FIG. 10I). In the tumor tissue, massive infiltrated CD3+ T cells accumulated in CpG2 vaccine applied group (FIG. 10J). Among the infiltrated CD8 T cells, a majority of them (around 40%) are OVA-specific CD8 T cells in CpG2 applied group, significantly more than CpG4 spacing at 7 nm (FIG. 10K). More IL-2+ CD8 T cells could be found in CpG2 group as well (FIG. 10L). The Gr-1+CD11b+ myeloid derived suppressive cells were found not increased in origami vaccine applied groups (FIG. 10M). These results indicated CpG spacing at 3.5 nm on SQB improved Th1 immune response in the treated tumor through a cohort of immune cell activation.

All references, patents and patent applications disclosed herein are incorporated by reference with respect to the subject matter for which each is cited, which in some cases may encompass the entirety of the document.

5 The indefinite articles “a” and “an,” as used herein in the specification and in the claims, unless clearly indicated to the contrary, should be understood to mean “at least one.”

It should also be understood that, unless clearly indicated to the contrary, in any methods claimed herein that include more than one step or act, the order of the steps or acts of the method is not necessarily limited to the order in which the steps or acts of the method are recited.

10 In the claims, as well as in the specification above, all transitional phrases such as “comprising,” “including,” “carrying,” “having,” “containing,” “involving,” “holding,” “composed of,” and the like are to be understood to be open-ended, i.e., to mean including but not limited to. Only the transitional phrases “consisting of” and “consisting essentially of” shall be closed or semi-closed transitional phrases, respectively, as set forth in the United States Patent Office Manual of Patent Examining Procedures, Section 2111.03.

15 The terms “about” and “substantially” preceding a numerical value mean $\pm 10\%$ of the recited numerical value.

Where a range of values is provided, each value between the upper and lower ends of the range are specifically contemplated and described herein.

What is claimed is:

CLAIMS

1. A nucleic acid nanostructure conjugated to an antigen, oligolysine-polyethylene glycol
5 copolymer, and CpG ligand, wherein the CpG ligand is uniformly spaced on the nucleic acid nanostructure.
2. The nucleic acid nanostructure of claim 1, wherein the distance between any two adjacent
10 molecules of CpG is 2 nm to 10 nm.
3. The nucleic acid nanostructure of claim 2, wherein the distance between any two adjacent
molecules of CpG is 2-3 nm, 3-4 nm, 4-6 nm, or 6-8 nm, optionally 2.5 nm, 3.5 nm, 5 nm, or 7
15 nm.
4. The nucleic acid nanostructure of any one of the preceding claims, wherein the density of
CpG ligand on the nucleic acid nanostructure is 1 molecule of CpG ligand per 5 to 50 nm².
5. The nucleic acid nanostructure of claim 3 or 4, wherein the distance between any two
20 adjacent molecules of CpG is 3.5 nm.
6. The nucleic acid nanostructure of claim 5, wherein the density of CpG ligand on the
nucleic acid nanostructure is 1 molecule of CpG ligand per 10 to 20 nm².
7. The nucleic acid nanostructure of claim 3 or 4, wherein the distance between any two
25 adjacent molecules of CpG is 5 nm.
8. The nucleic acid nanostructure of claim 7, wherein the density of CpG ligand on the
nucleic acid nanostructure is 1 molecule of CpG ligand per 20 to 30 nm².
9. The nucleic acid nanostructure of any one of the preceding claims, wherein the nucleic
30 acid nanostructure comprises a square-lattice structure.
10. The nucleic acid nanostructure of claim 9, wherein the CpG ligand is located on at least
one surface of the nucleic acid nanostructure.

11. The nucleic acid nanostructure of claim 9 or 10, wherein the antigen is located on at least one surface of the nucleic acid nanostructure.
12. The nucleic acid nanostructure of claim 10 or 11, wherein the CpG ligand and the antigen
5 are located on different surfaces of the nucleic acid nanostructure, relative to each other.
13. The nucleic acid nanostructure of any one of the preceding claims, wherein the nucleic acid nanostructure comprises 5 to 25, 10 to 25, or 15 to 25 CpG ligand molecules.
- 10 14. The nucleic acid nanostructure of any one of the preceding claims, wherein the CpG ligand and/or antigen are located on a single surface of the nucleic acid nanostructure.
15. The nucleic acid nanostructure of any one of the preceding claims, wherein the oligolysine-polyethylene glycol (PEG) copolymer comprises ten lysine residues and five PEG
15 molecules (K10PEG5).
16. The nucleic acid nanostructure of any one of the preceding claims, wherein the oligolysine- PEG copolymer consists of K10PEG5.
- 20 17. The nucleic acid nanostructure of any one of the preceding claims, wherein the antigen is covalently conjugated to the nanostructure.
18. The nucleic acid nanostructure of any one of the preceding claims, wherein the oligolysine-PEG copolymer is covalently conjugated to the nanostructure.
25
19. The nucleic acid nanostructure of any one of the preceding claims, wherein the nucleic acid of the nanostructure comprises DNA, RNA, or a mixture of DNA and RNA.
20. The nucleic acid nanostructure of claim 18, wherein the nucleic acid of the nanostructure
30 comprises DNA.
21. The nucleic acid nanostructure of claim 19, wherein the nucleic acid of the nanostructure consists of DNA.

22. A DNA nanostructure conjugated to an antigen, oligolysine-polyethylene glycol copolymer, and CpG ligand, wherein the DNA nanostructure comprises a square-lattice structure, the CpG ligand is uniformly spaced with a density of 1 molecule of CpG ligand per 10-30 nm², and the distance between any two adjacent molecules of CpG is 3-5 nm.

5

23. A method comprising delivering to a subject the nanostructure of any one of the preceding claims in an effective amount to produce a CD8+ T cell immune response in the subject.

10 24. The method of claim 23, wherein the subject has a tumor.

25. The method of claim 24, wherein the antigen is a tumor antigen.

15 26. The method of any one of the preceding claims, wherein administration of the nanostructure results in an at least 2-fold or at least 3-fold reduction in tumor volume.

27. The method of any one of the preceding claims, wherein administration of the nanostructure stimulates cytokine production in dendritic cells of the subject, wherein the cytokine production is at least 10%, at least 15%, or at least 20% higher than cytokine
20 production by dendritic cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

28. The method of claim 27, wherein administration of the nanostructure stimulates Interleukin-10 (IL10) and/or IL12 production in dendritic cells of the subject.

25

29. The method of any one of the preceding claims, wherein administration of the nanostructure increases antigen uptake in dendritic cells of the subject, wherein the antigen uptake is at least 10%, at least 15%, or at least 20% higher than antigen uptake by dendritic cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

30

30. The method of any one of the preceding claims, wherein administration of the nanostructure stimulates a stronger Th1 immune response, relative to stimulation of a Th2 response.

31. The method of claim 30, wherein the Th1 immune response is characterized by expression of CD69 and CD8 on T cells.

32. The method of any one of the preceding claims, wherein administration of the
5 nanostructure stimulates CD8+ T cell proliferation by at least 10%, at least 15%, or at least 20% relative to CD8+ T cell proliferation in control cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

33. The method of any one of the preceding claims, wherein administration of the
10 nanostructure stimulates IFN- γ expression in OT-I CD8+ T cells of the subject, wherein the IFN- γ expression is at least 10%, at least 15%, or at least 20% higher than IFN- γ expression by in OT-I CD8+ T cells in a subject administered antigen only or antigen and free CpG oligonucleotides.

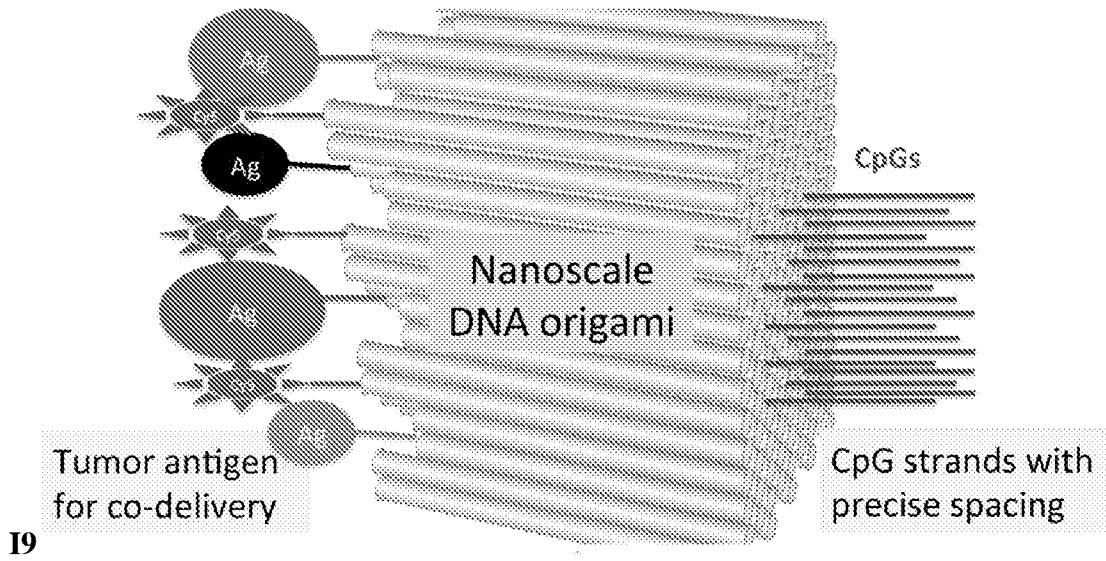


FIG. 1

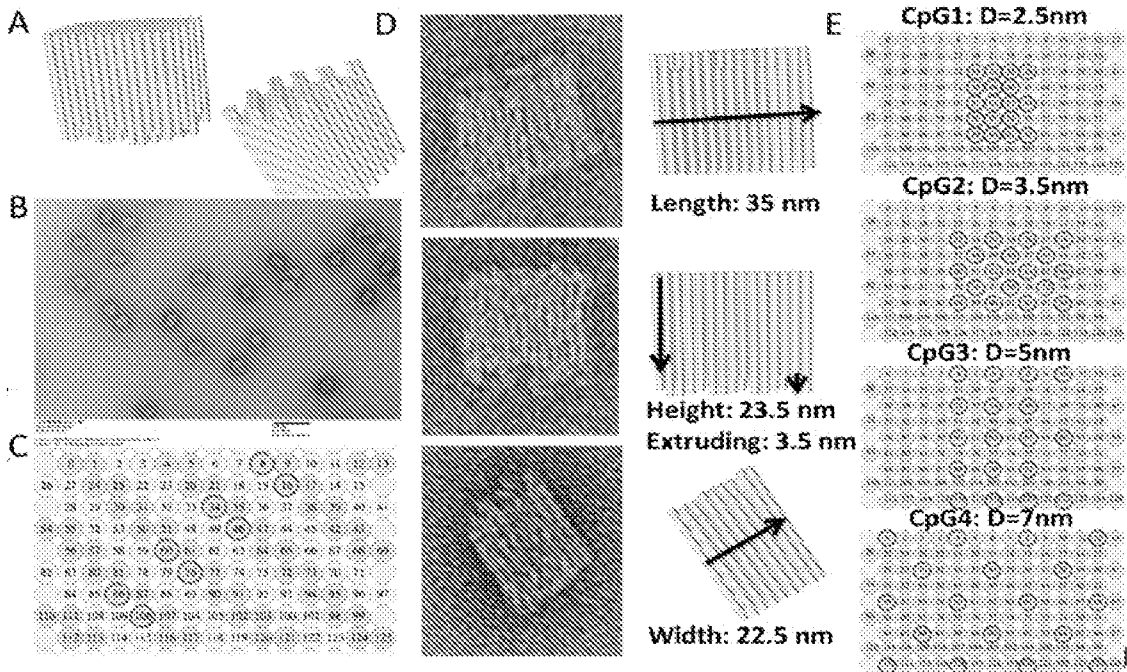


FIG. 2

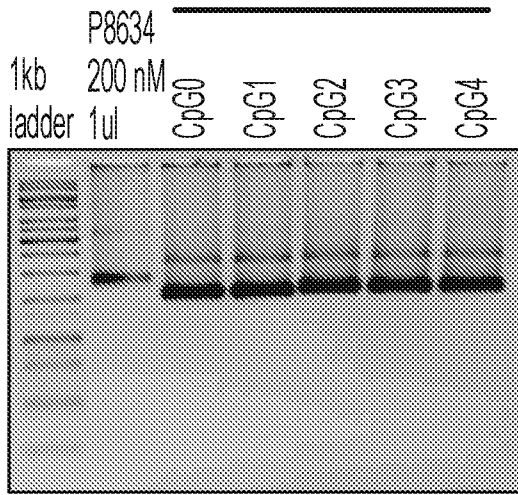


FIG. 3A

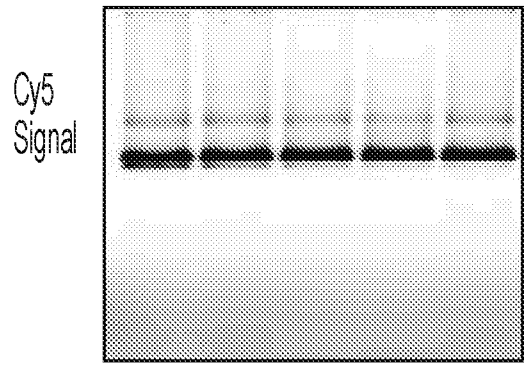


FIG. 3B

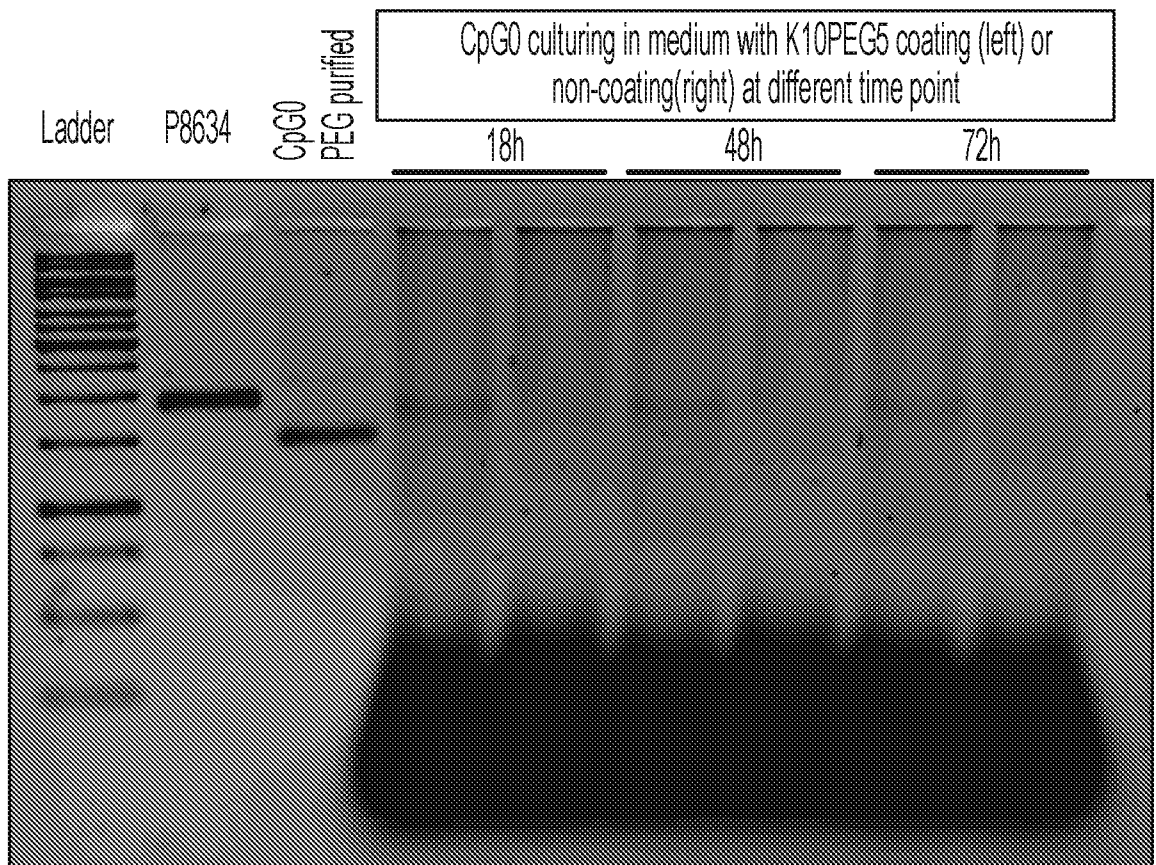


FIG. 3C

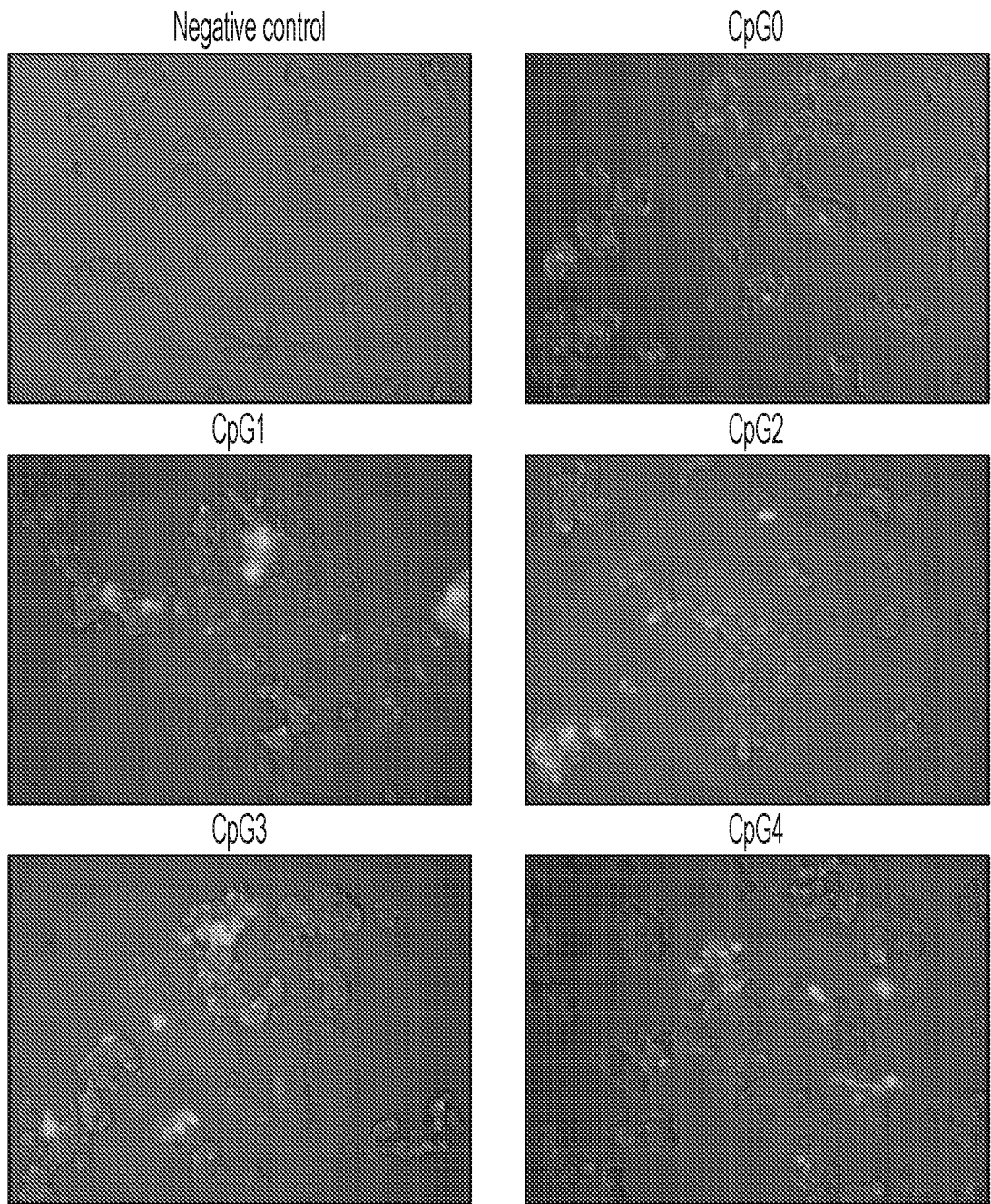


FIG. 3D

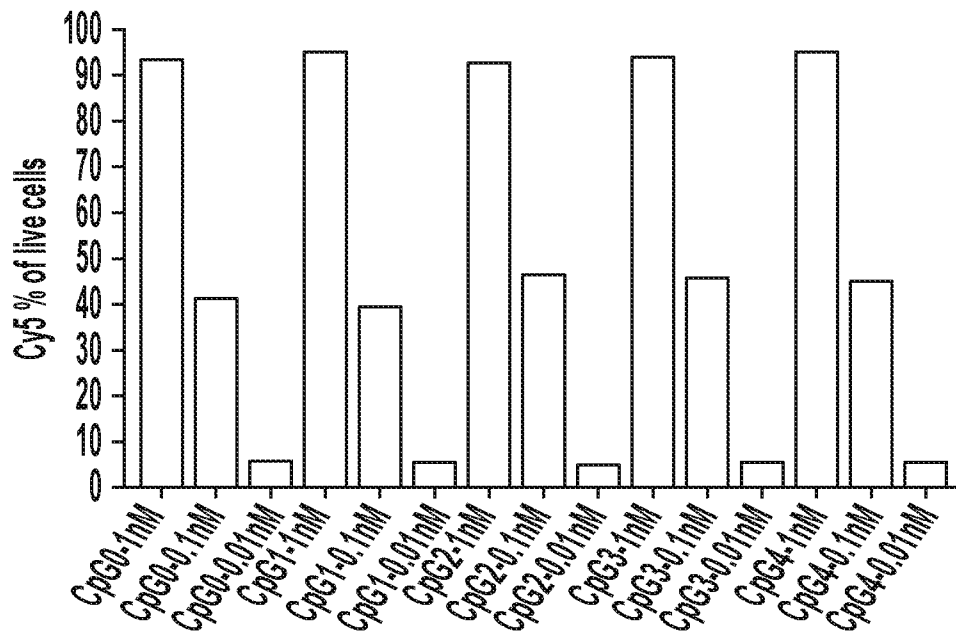


FIG. 3E

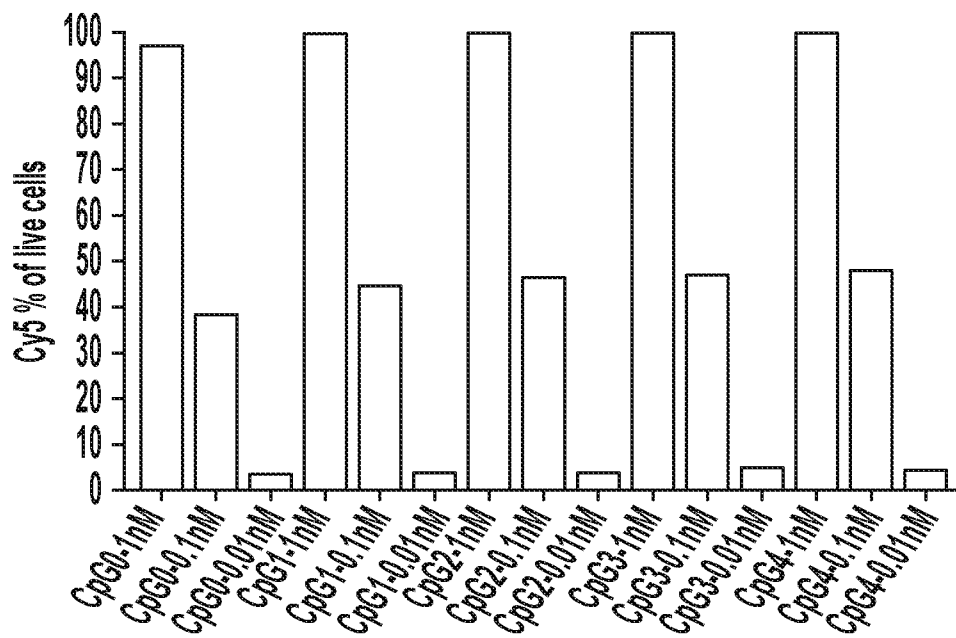


FIG. 3F

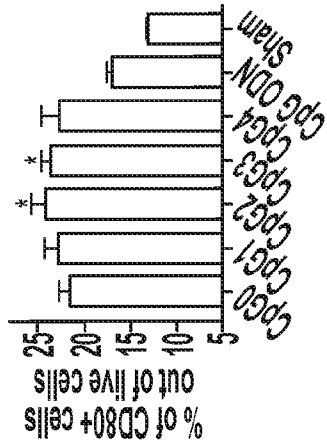


FIG. 4C

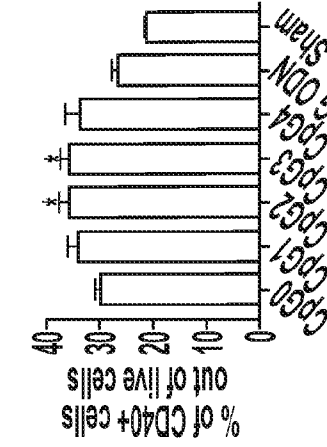


FIG. 4D

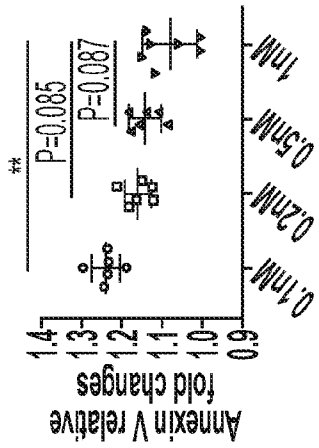


FIG. 4E

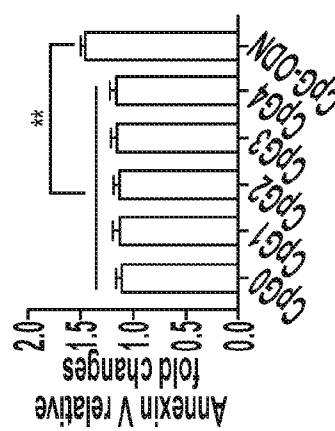


FIG. 4F

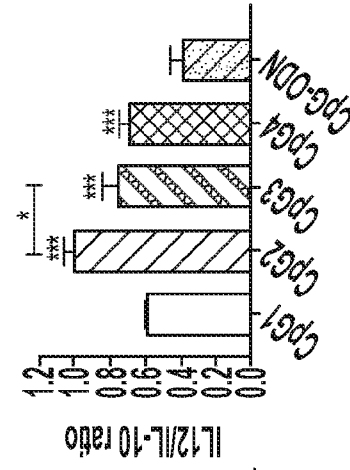


FIG. 4G

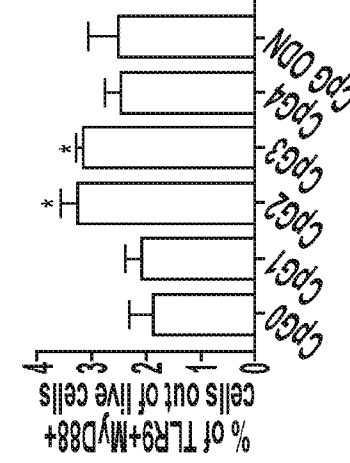


FIG. 4H

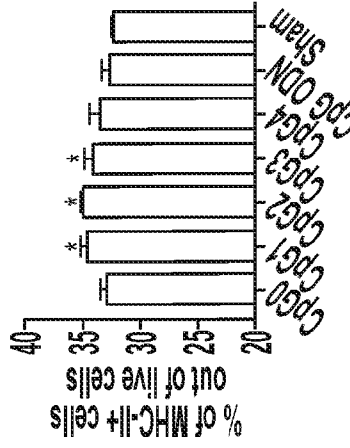


FIG. 4I

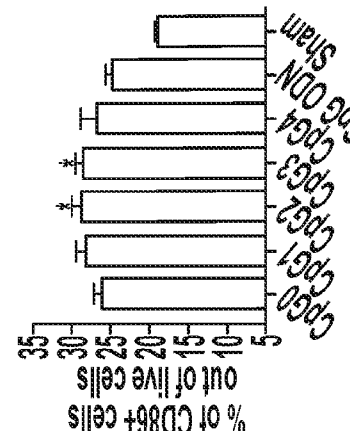


FIG. 4J

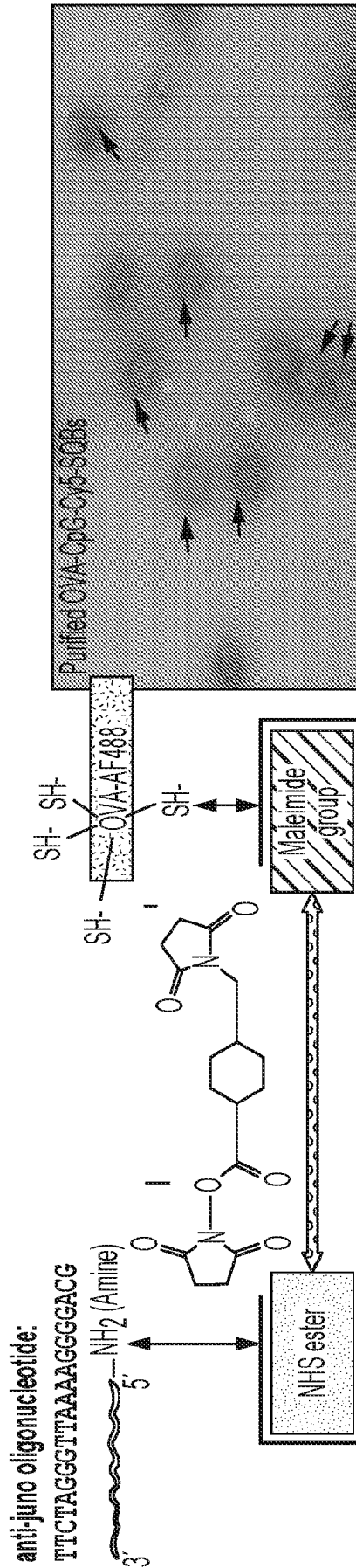


FIG. 5A

FIG. 5B

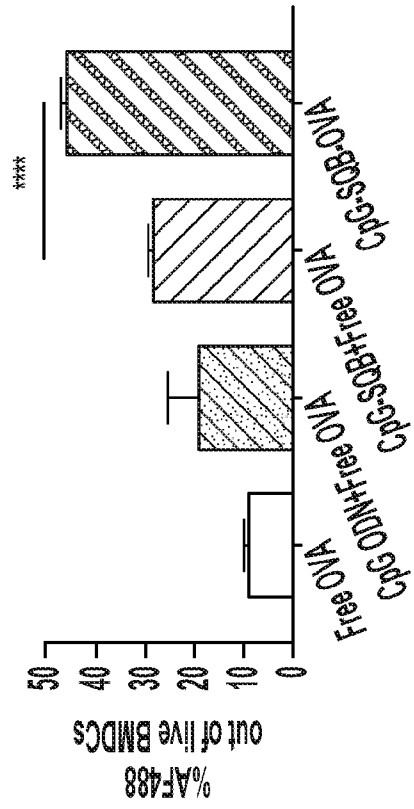


FIG. 5C

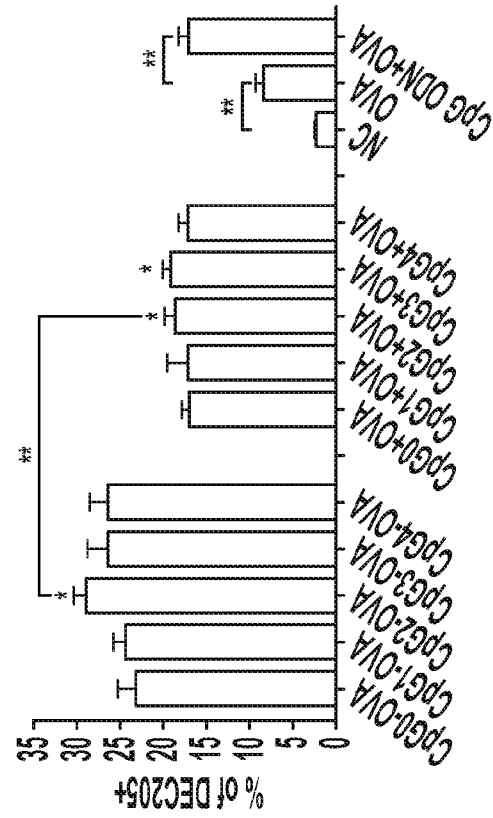


FIG. 5D

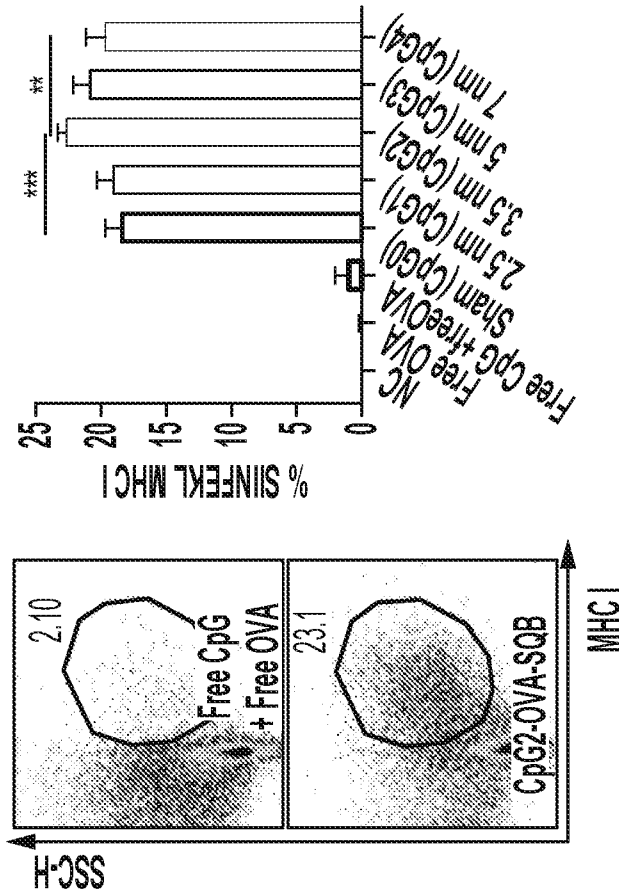


FIG. 5F

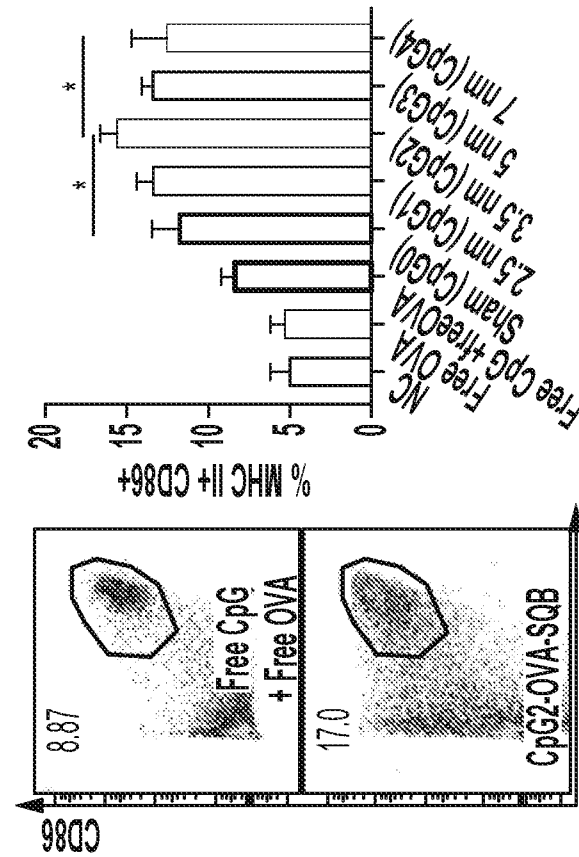


FIG. 5E

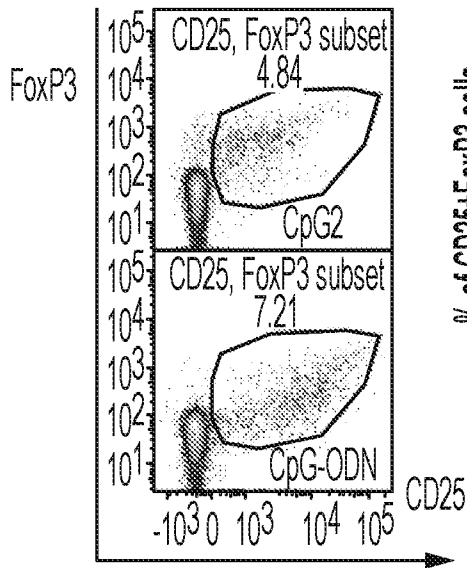


FIG. 6A

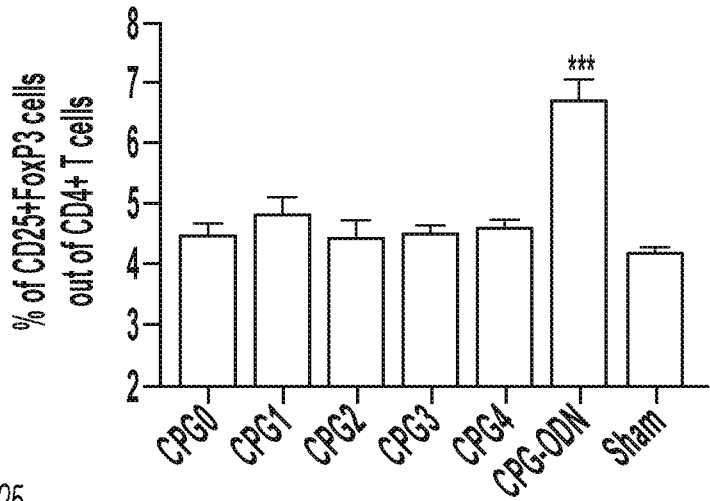


FIG. 6B

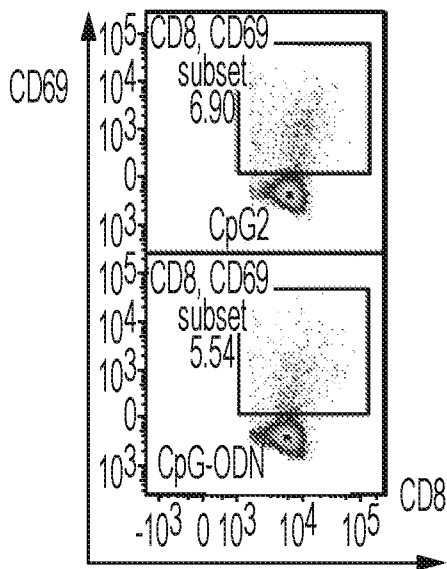


FIG. 6C

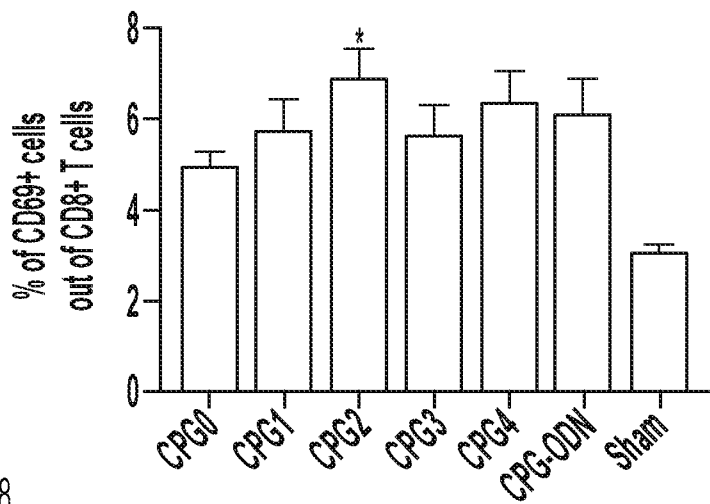


FIG. 6D

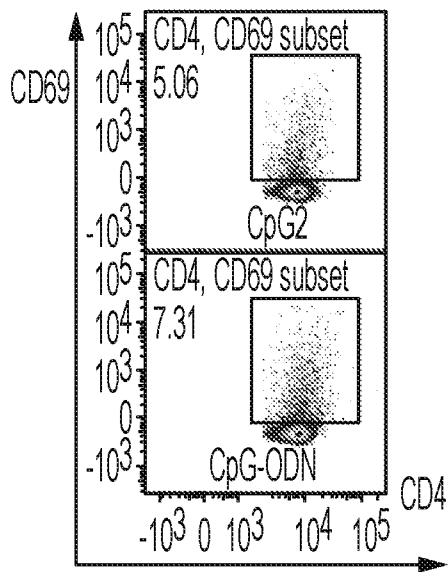


FIG. 6E

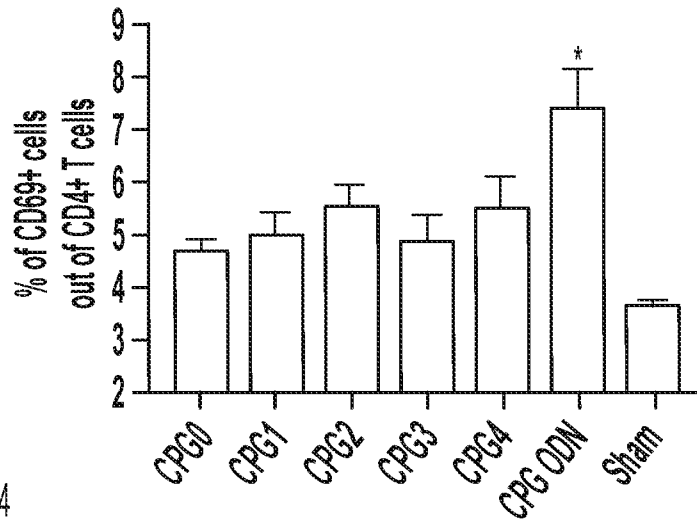


FIG. 6F

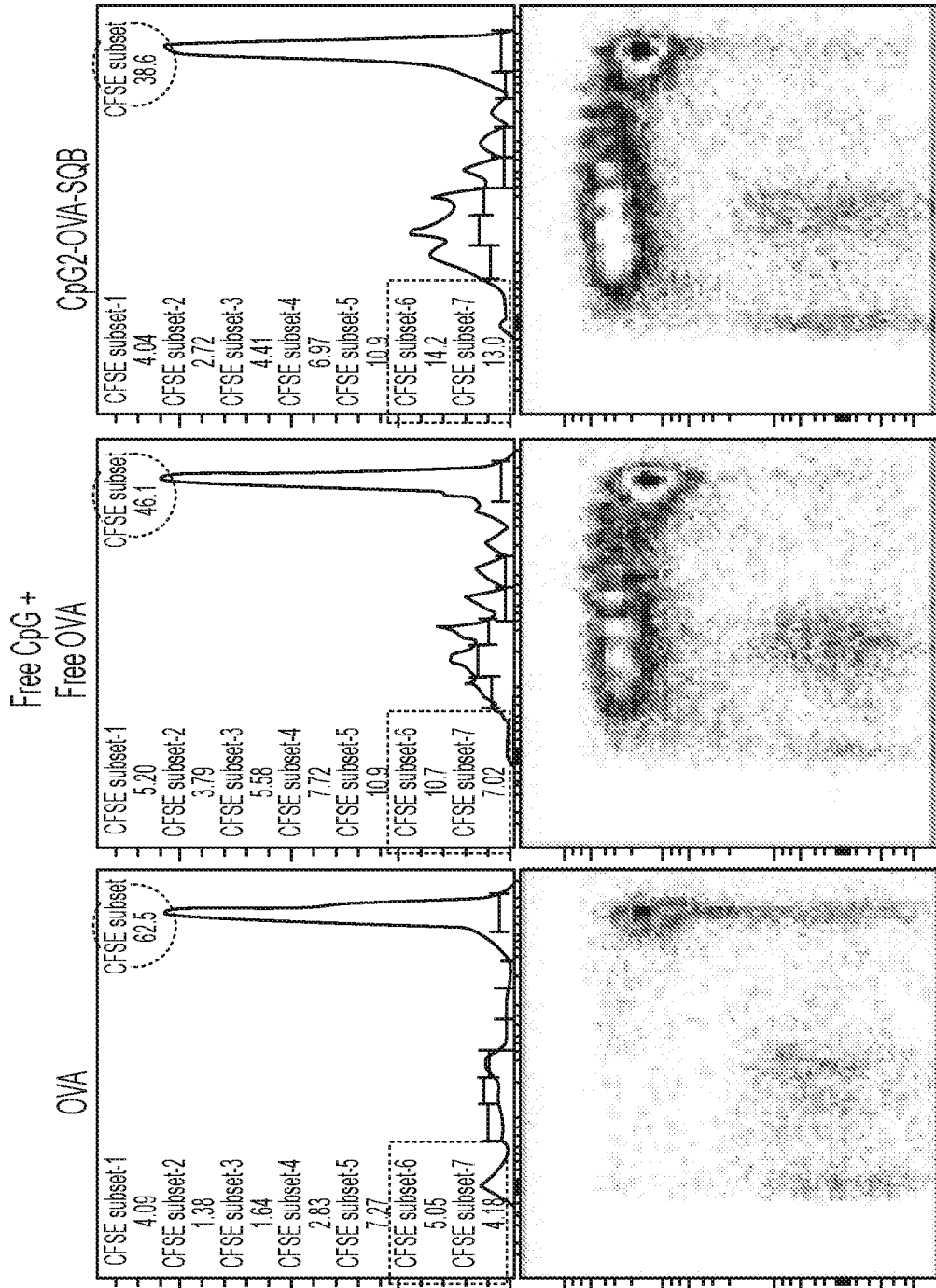


FIG. 7A

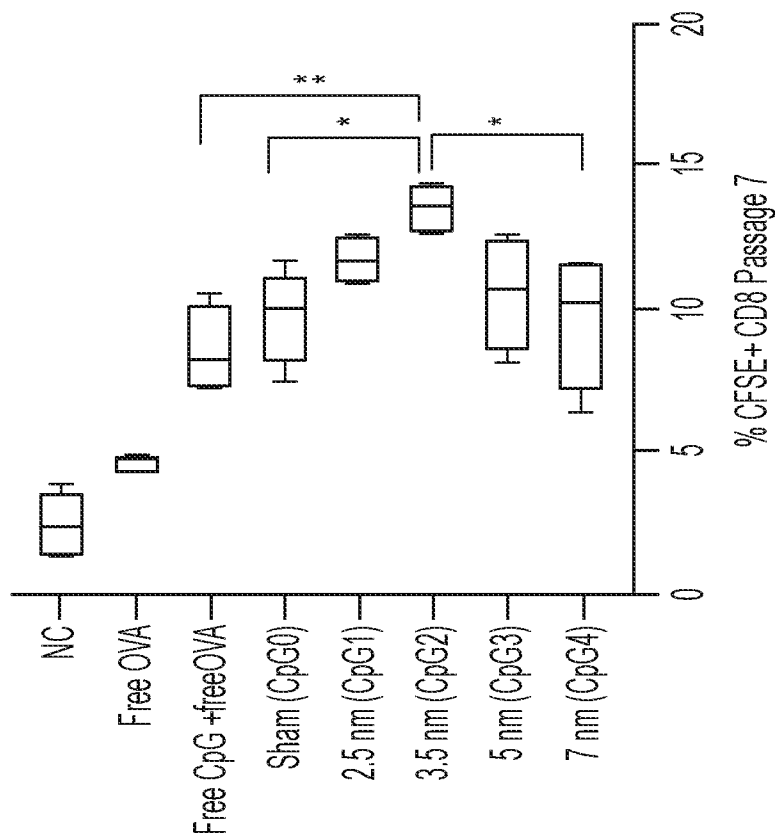


FIG. 7B

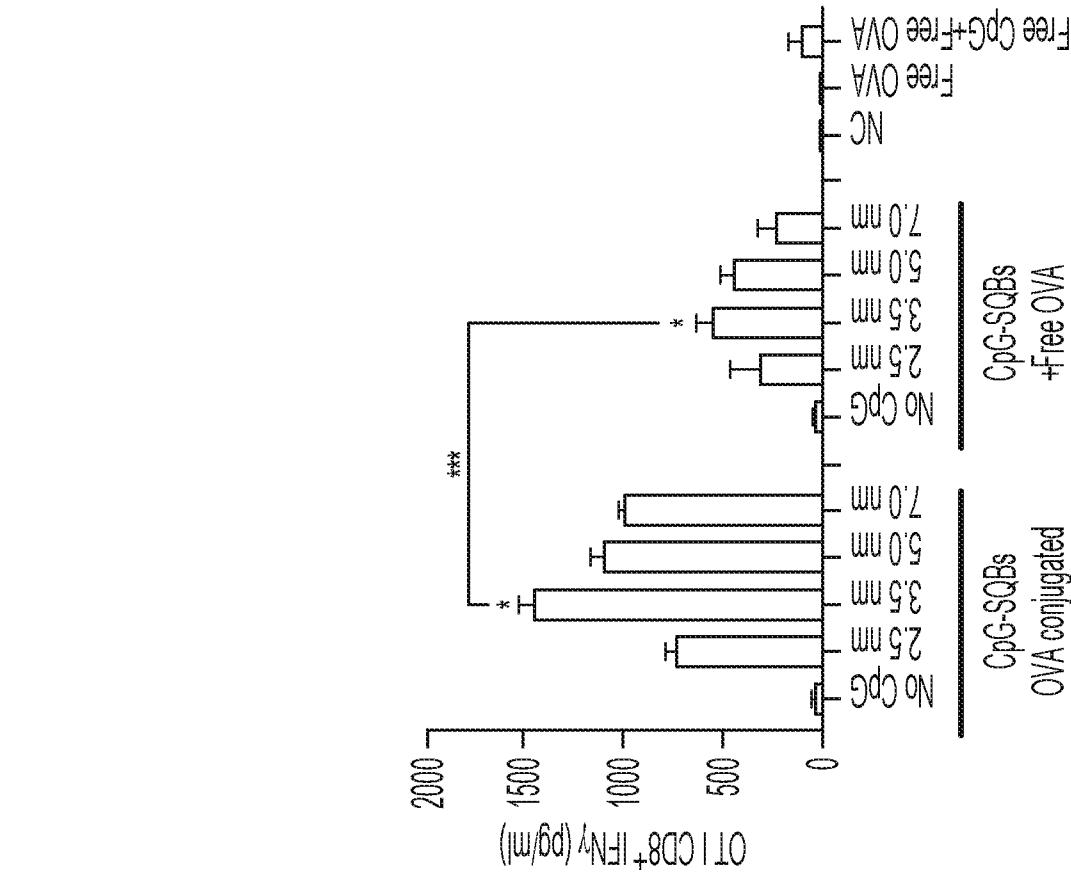


FIG. 7C

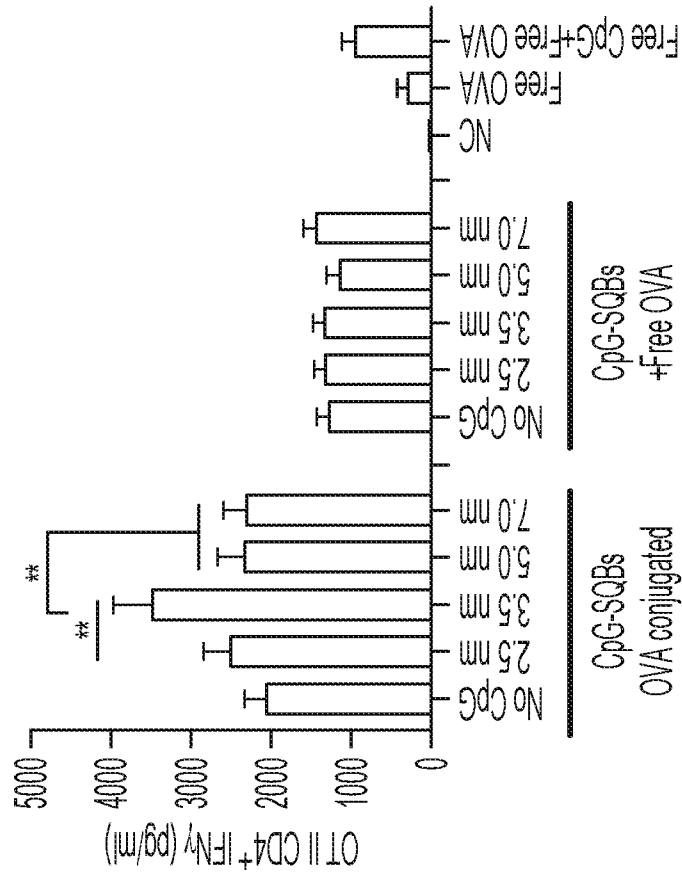


FIG. 7E

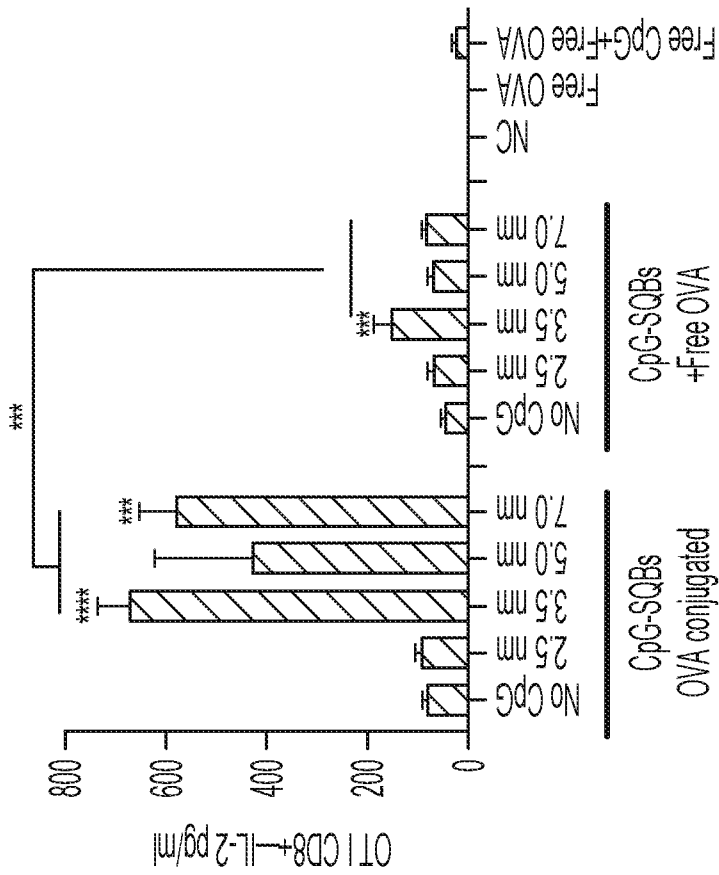


FIG. 7D

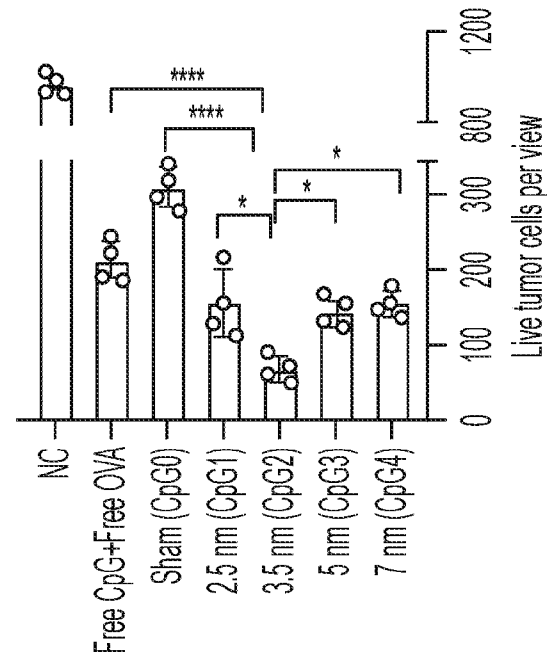


FIG. 7G

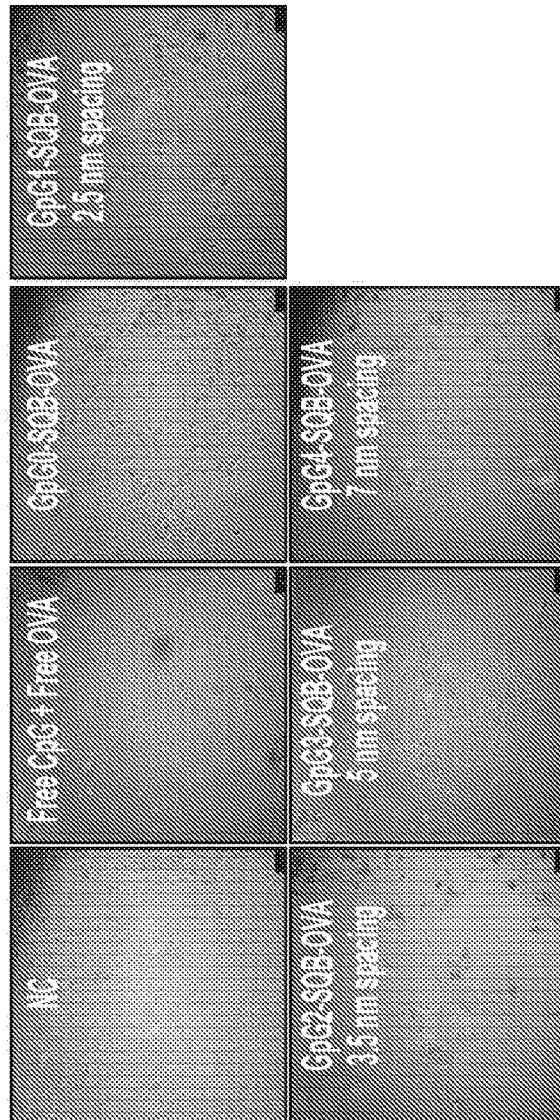
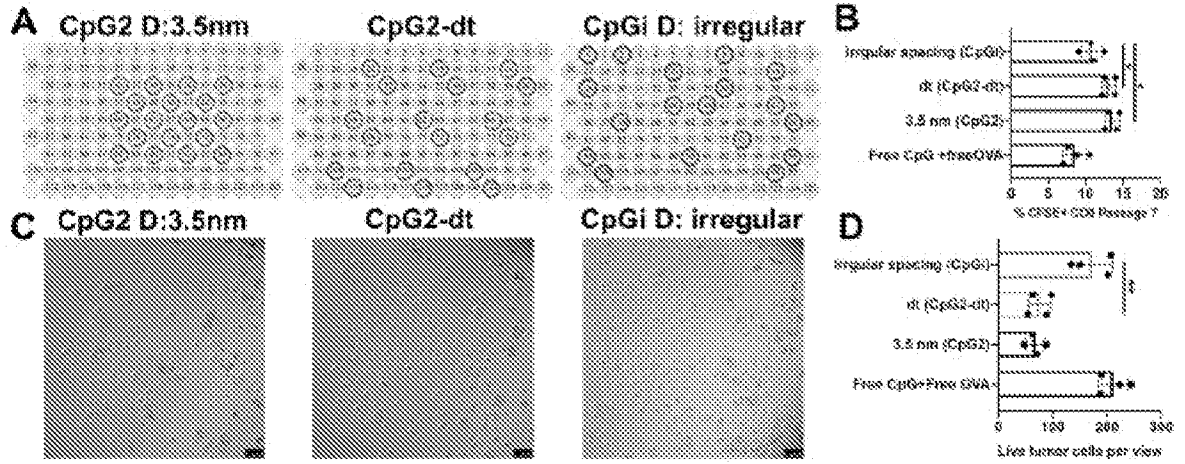


FIG. 7F



FIGS. 8A-8D

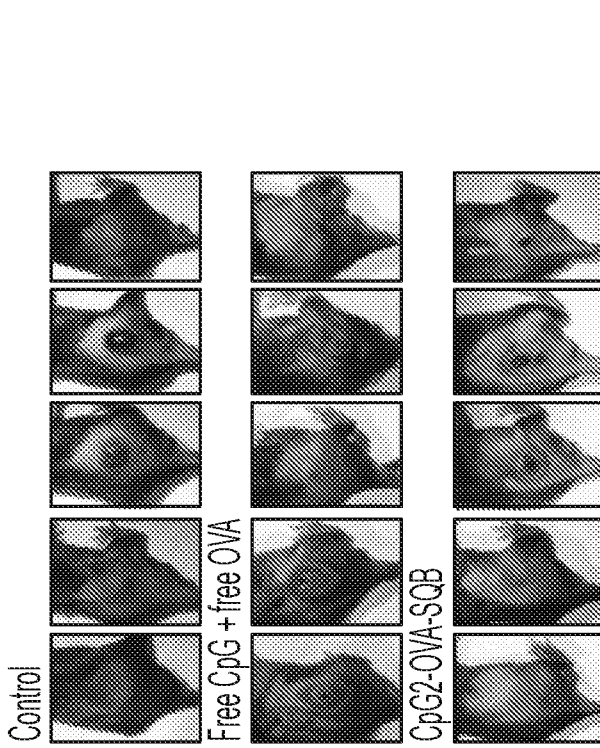


FIG. 9B

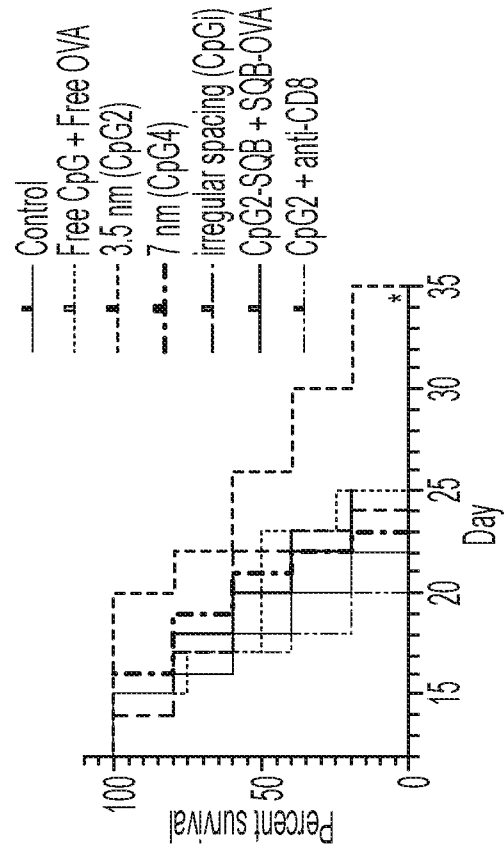


FIG. 9D

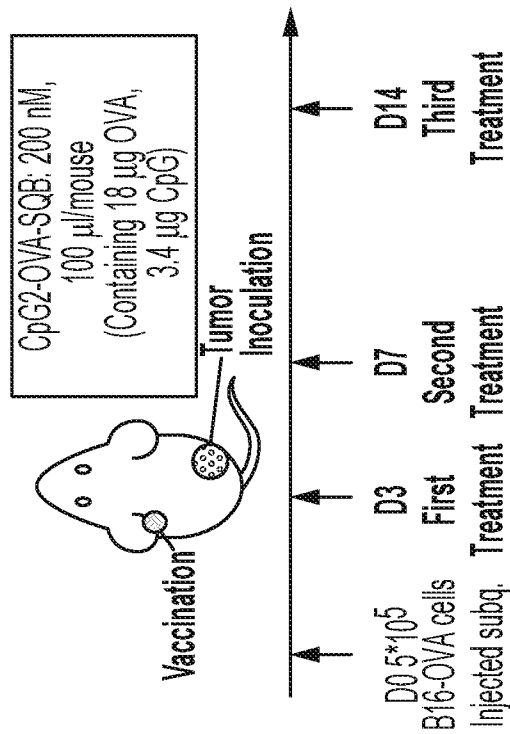


FIG. 9A

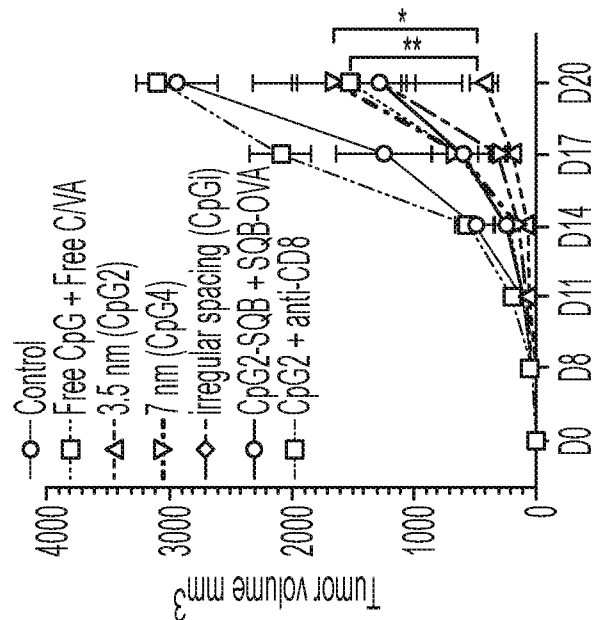


FIG. 9C

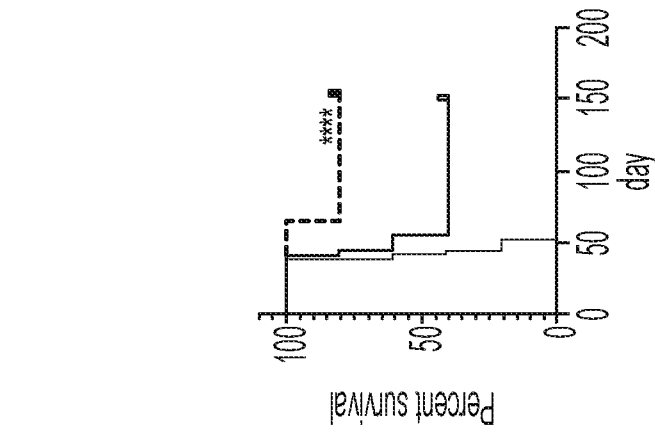


FIG. 9G

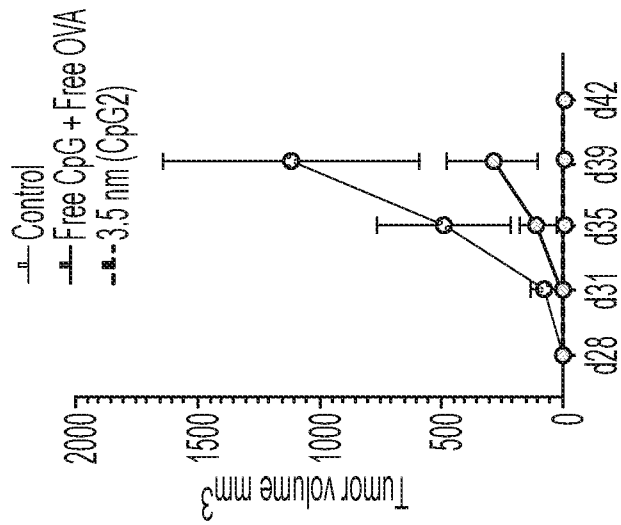


FIG. 9F

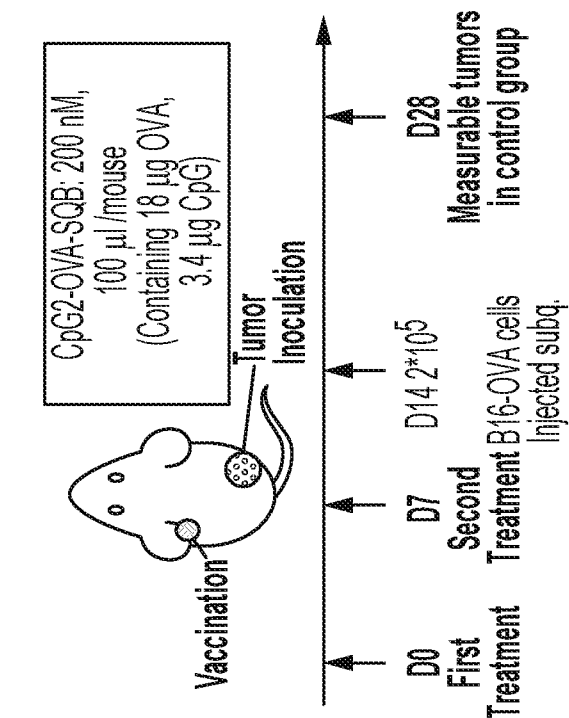


FIG. 9E

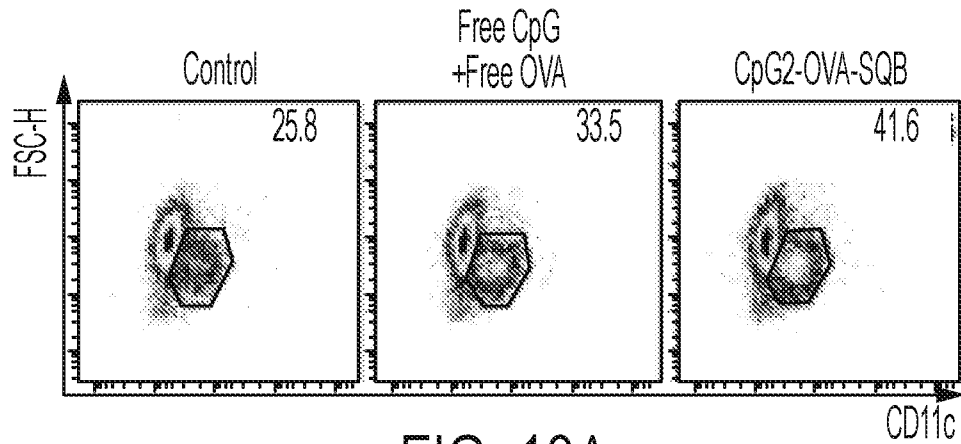


FIG. 10A

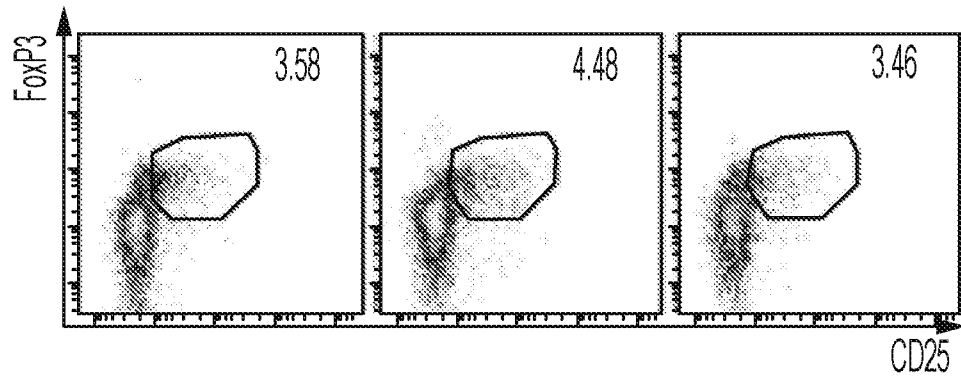


FIG. 10B

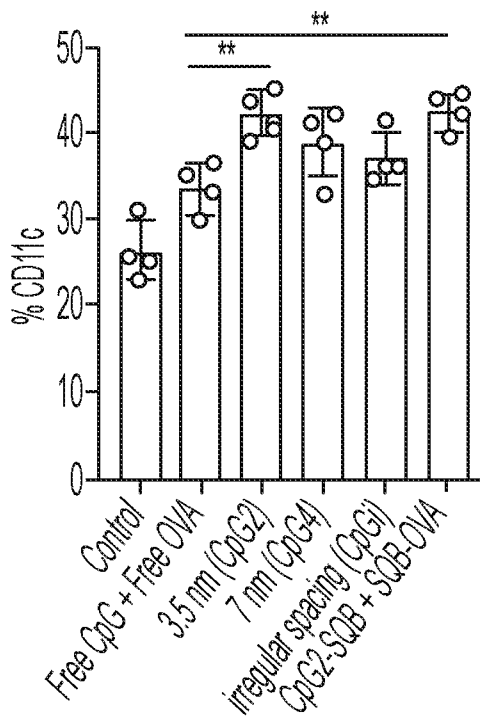


FIG. 10C

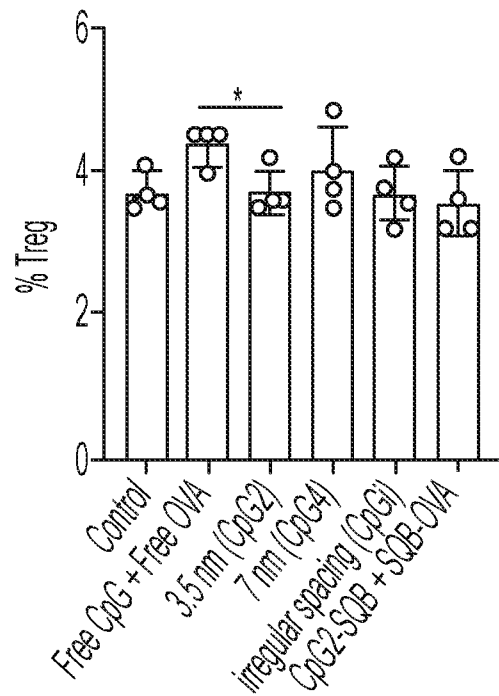


FIG. 10D

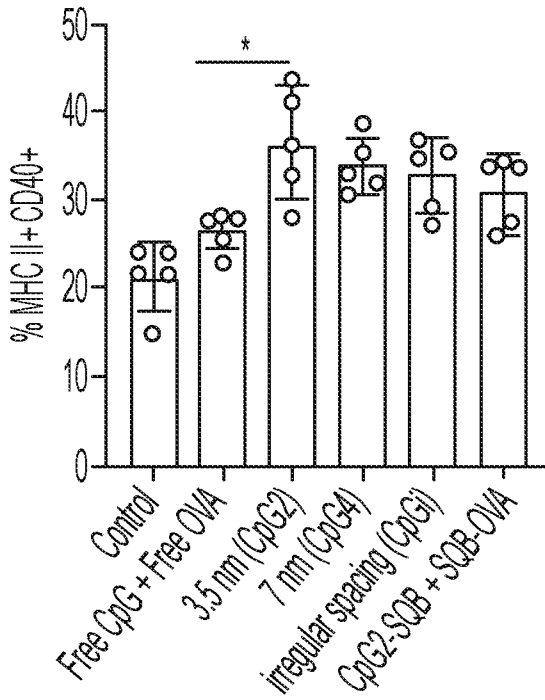


FIG. 10E

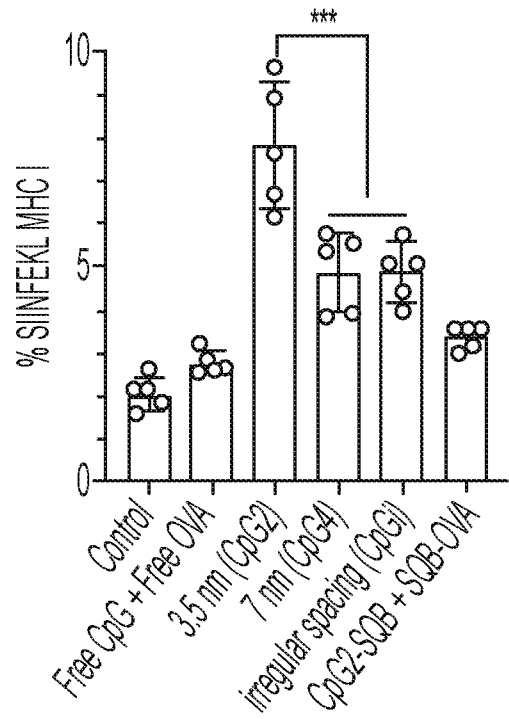


FIG. 10F

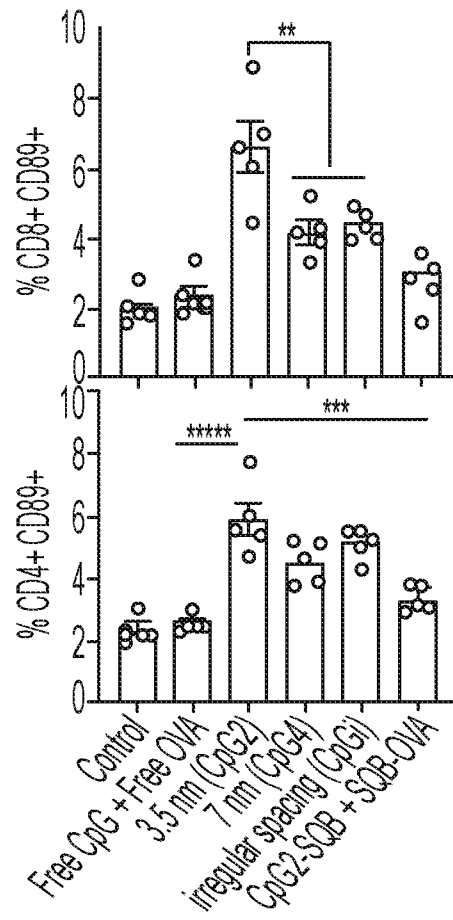
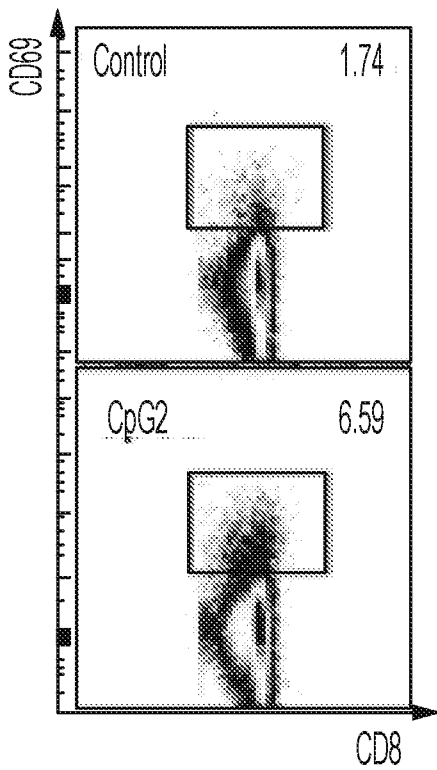


FIG. 10G

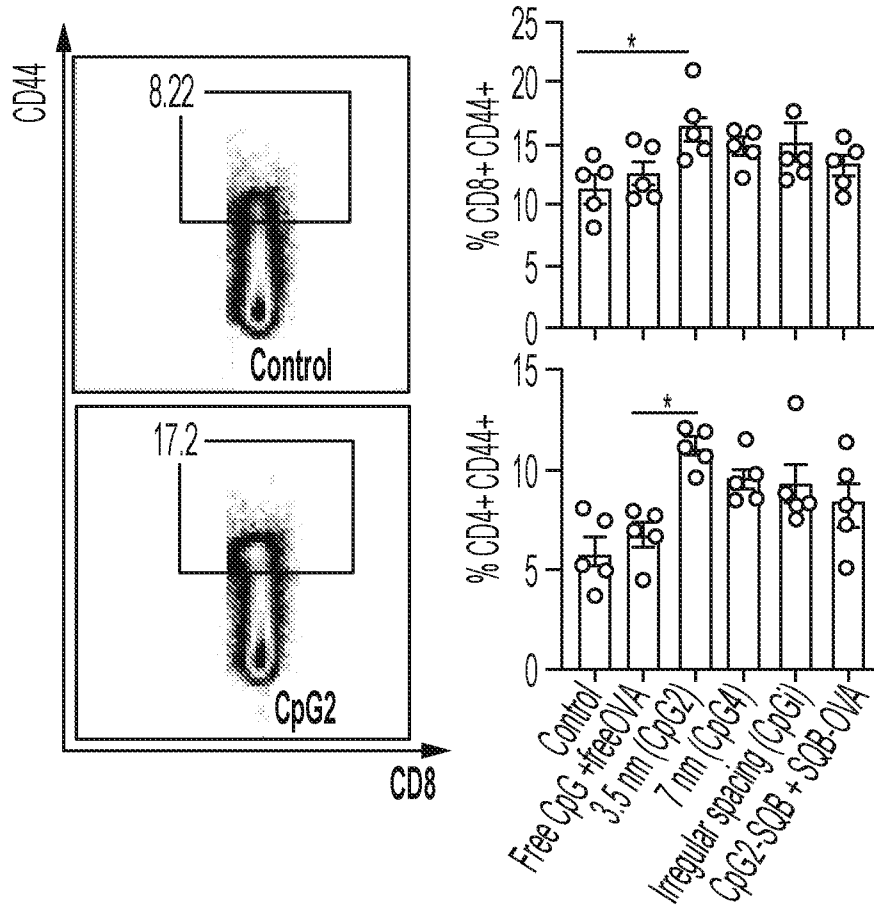


FIG. 10H

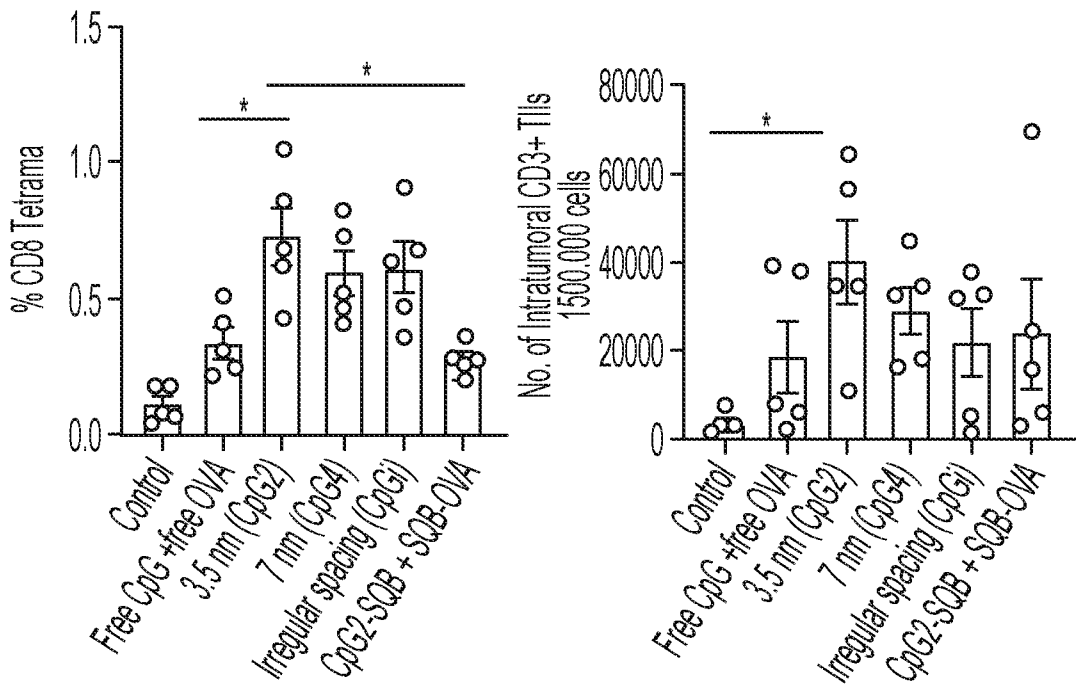


FIG. 10I

FIG. 10J

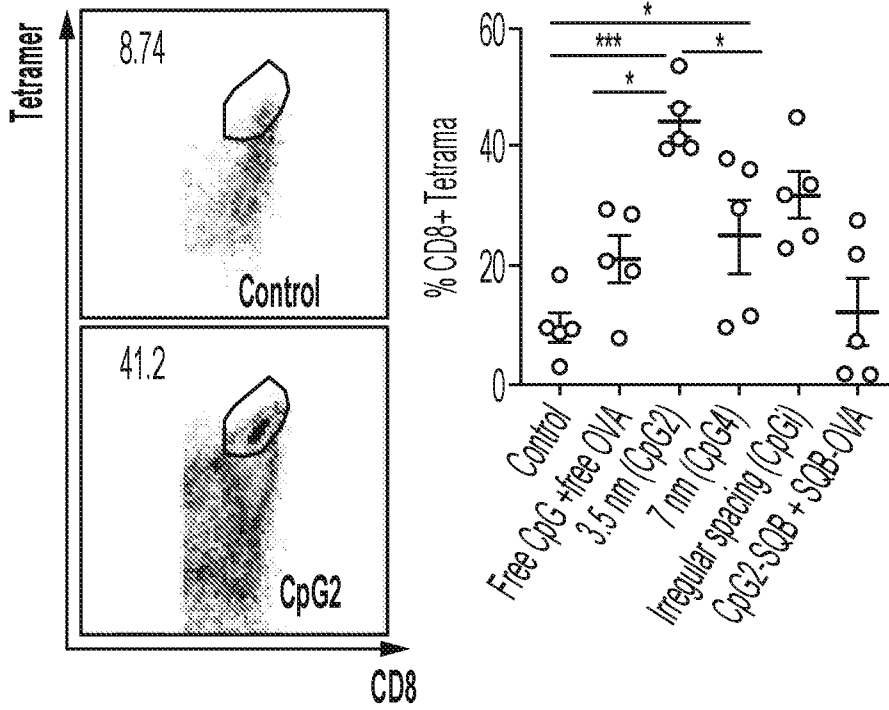


FIG. 10K

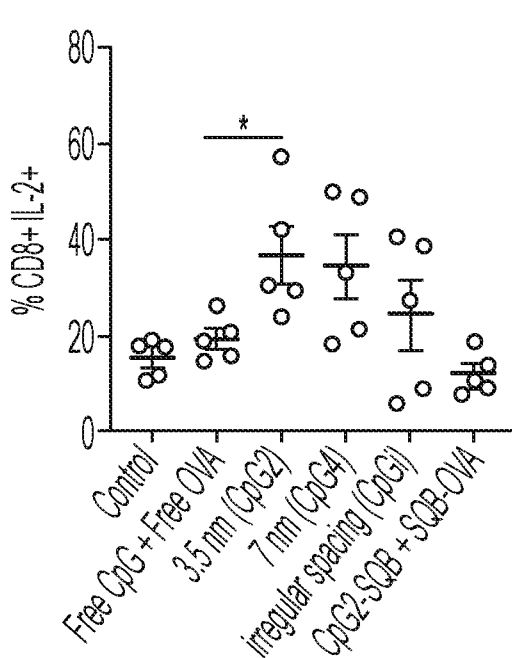


FIG. 10L

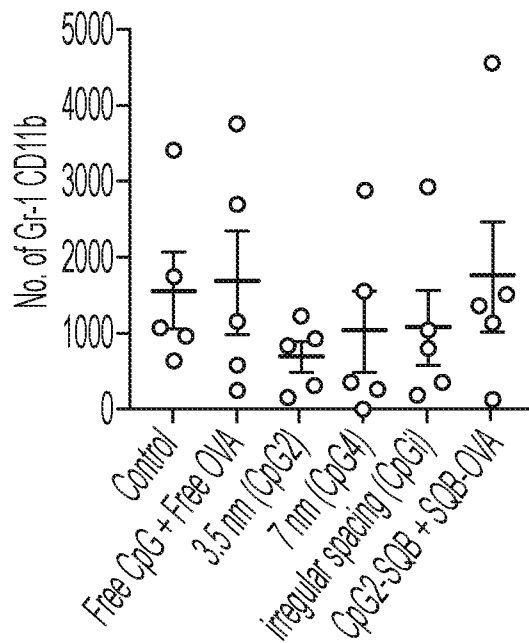


FIG. 10M

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 20/36281

A. CLASSIFICATION OF SUBJECT MATTER

IPC - A61K 39/39; A61K 31/711; A61K 47/10; B82Y 5/00; C07H 21/04 (2020.01)

CPC - A61K 39/39; A61K 31/711; A61K 2039/5561; A61K 47/645; A61K 47/10; B82Y 5/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
See Search History document

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched
See Search History document

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
See Search History document

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2016/0271268 A1 (DANA FARBER CANCER INSTITUTE, INC.) 22 September 2016 (22.09.2016) para [0063], [0085], [0099], [0180], [0254], sheet 18 fig 17, sheet 26 fig 22B.	1-4, 22
A	LI et al. Self-assembled multivalent DNA nanostructures for noninvasive intracellular delivery of immunostimulatory CpG oligonucleotides. ACS Nano, 22 November 2011, Vol 5, No 11, Pages 8783-8789. Especially abstract, Supporting Information Figure S1, Table S1.	1-4, 22
A	WO 2017/189870 A1 (MASSACHUSETTS INSTITUTE OF TECHNOLOGY) 2 November 2017 (02.11.2017) claims 1-47	1-4, 22

Further documents are listed in the continuation of Box C. See patent family annex.

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"D" document cited by the applicant in the international application	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"E" earlier application or patent but published on or after the international filing date	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	"&" document member of the same patent family
"O" document referring to an oral disclosure, use, exhibition or other means	
"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search
10 September 2020

Date of mailing of the international search report
30 SEP 2020

Name and mailing address of the ISA/US
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Facsimile No. 571-273-8300

Authorized officer
Lee Young
Telephone No. PCT Helpdesk: 571-272-4300

INTERNATIONAL SEARCH REPORT

International application No.

PCT/US 20/36281

Box No. II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)

This international search report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

- 1. Claims Nos.:
because they relate to subject matter not required to be searched by this Authority, namely:

- 2. Claims Nos.:
because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

- 3. Claims Nos.: 5-21, 23-33
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box No. III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

- 1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
- 2. As all searchable claims could be searched without effort justifying additional fees, this Authority did not invite payment of additional fees.
- 3. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:

- 4. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

- Remark on Protest**
- The additional search fees were accompanied by the applicant's protest and, where applicable, the payment of a protest fee.
 - The additional search fees were accompanied by the applicant's protest but the applicable protest fee was not paid within the time limit specified in the invitation.
 - No protest accompanied the payment of additional search fees.