



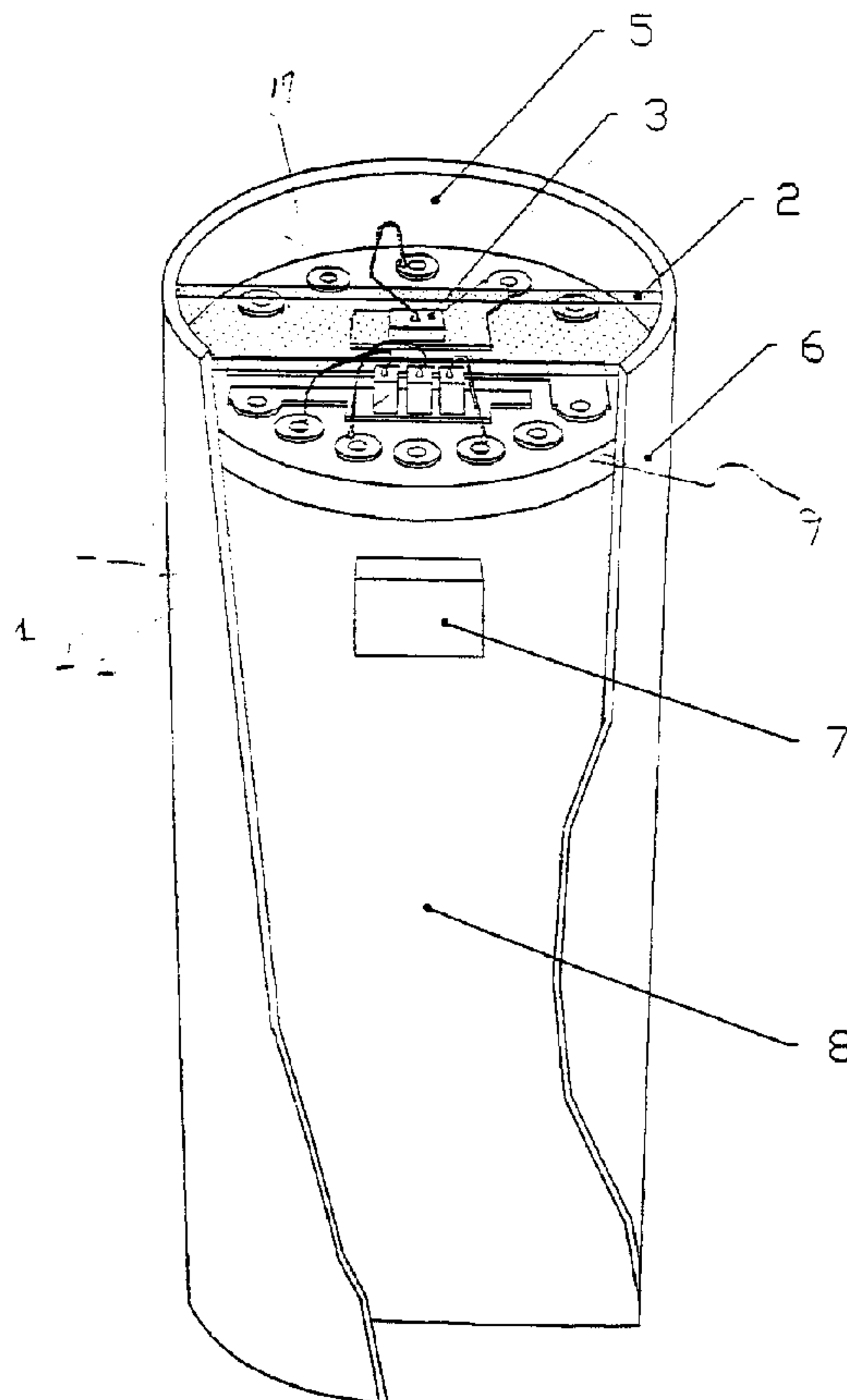
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(54) **SONDE HYBRIDE DE RECONNAISSANCE DE TYPE DE TISSU**

(54) **HYBRID PROBE FOR TISSUE TYPE RECOGNITION**



(57) L'invention concerne une sonde hybride dans laquelle les trajets et capteurs optiques comprennent des éléments placés à l'intérieur d'une structure à microplaquette, hybride et compacte, le système optique complet (1, 2, 3) de cette sonde hybride étant disposé au

(57) This invention is a hybrid probe in which the optical pathways and the optical sensors comprise elements located within a compact hybrid chip structure. The full optical system (1, 2, 3) of the hybrid probe is located at its tip. No fibers are required to bring the light to and



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bout de celle-ci. Aucune fibre optique n'est nécessaire pour diriger la lumière depuis ou vers le bout de ladite sonde, une ou plusieurs puces à diodes électroluminescentes (1) étant montées sur un substrat (9), situé au bout de cette sonde. Les raccords appropriés sont effectués sur ces puces, qui sont alimentées par des dispositifs électroniques situés sur la poignée de ladite sonde.

from the tip of the probe. This is achieved in part by mounting one or more LED dice (1) on a substrate (9) at the probe tip. Appropriate connections are made to these dice which are powered from electronics in the handle of the probe.

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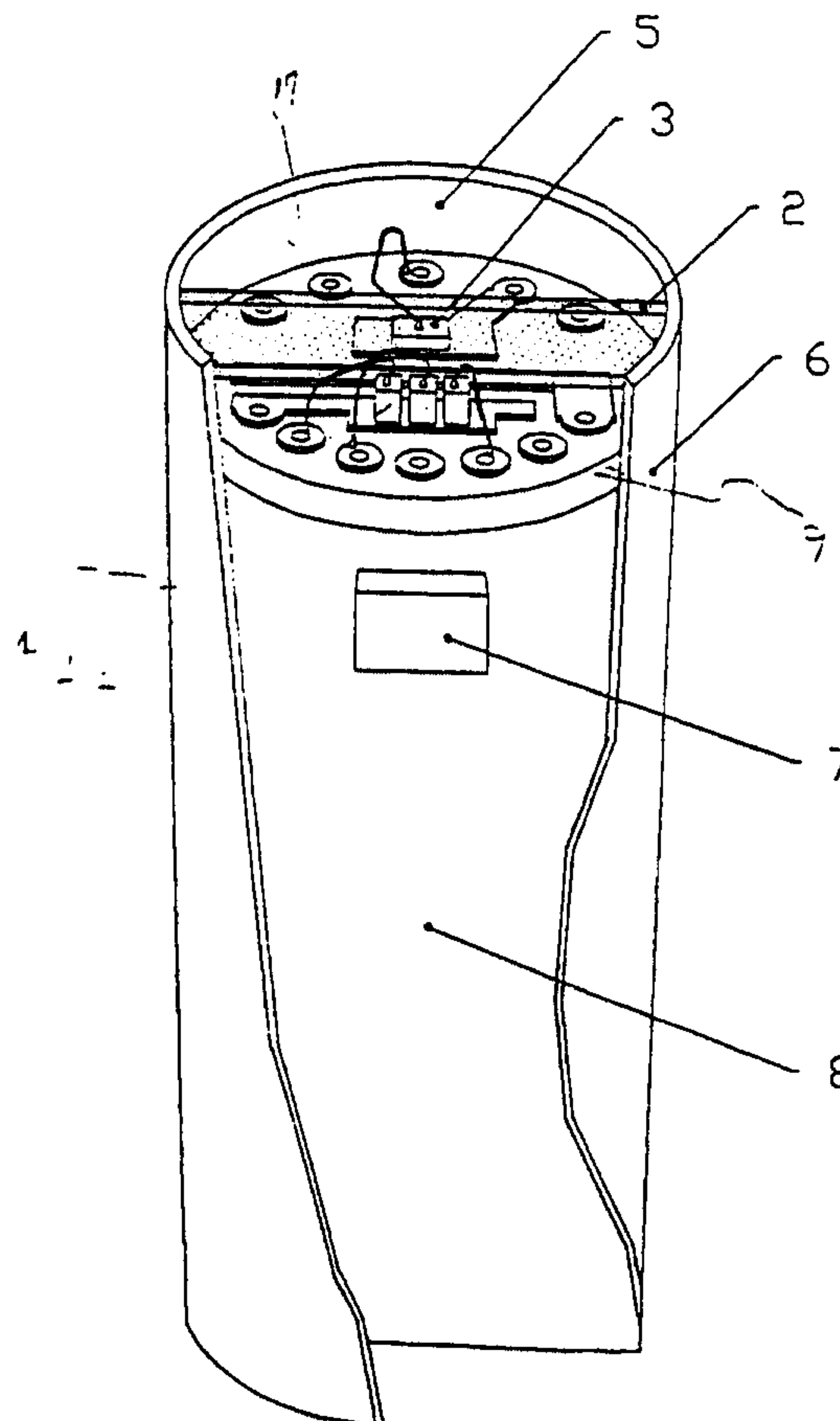
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(54) Title: HYBRID PROBE FOR TISSUE TYPE RECOGNITION

(57) Abstract

This invention is a hybrid probe in which the optical pathways and the optical sensors comprise elements located within a compact hybrid chip structure. The full optical system (1, 2, 3) of the hybrid probe is located at its tip. No fibers are required to bring the light to and from the tip of the probe. This is achieved in part by mounting one or more LED dice (1) on a substrate (9) at the probe tip. Appropriate connections are made to these dice which are powered from electronics in the handle of the probe.



HYBRID PROBE FOR TISSUE TYPE RECOGNITION**FIELD OF THE INVENTION**

5 The present invention relates to probes
and a method for identifying different tissue
types including those displaying modifications
involving pre-cancerous and cancerous stages,
diseased tissue, and those that are in a
transitional stage.

10 The identification of different tissue
types is provided via a set of measurements of
the tissue's physical properties and in
particular the optical and electrical
properties of the tissue.

15

BACKGROUND OF THE INVENTION

 The medical profession often needs to have
an objective assessment of the health of the
tissue of a patient. The patient may have
20 suffered tissue damage as a result of
accidental or deliberate trauma as for example
during a surgical operation. The patient may
also be suffering some other more persistent
irritation as a result, for example, of being
25 confined to bed which can lead to bed sores.
It is valuable for a medical practitioner to be
able to tell in advance the type of treatment
that would benefit the patient.

 It is well known, for example, that early
30 detection of tissues displaying pre-cancer or
cancer modifications is important for success-
ful medical treatment. We have already dis-
closed an apparatus and method for carrying out
this detection. The invention described in
35 this application represents a significant im-
provement on the apparatus disclosed in patent
application S.N. 08/332,830, assigned to the

same assignee as the current invention.

The previous disclosure described an apparatus that employed optical fibre technology for performing the optical measurements.

5 While this technology is effective, a good deal of manual labor is involved in building a probe to that design. The level of skill required precludes the manufacture of the device on a large scale at a low price for a mass market.

10 The fibre-based device also has potential problems with temperature sensitivity which cannot be avoided with optical fibers, particularly when they are bent and the temperature sensitivity cannot readily be compensated.

15 Close spacing of opto-electronics components is typically avoided in diagnostic probe design because of the difficulties of providing adequate electrical and optical isolation. Optical fibers are often used to
20 enable the opto-electronics components to be held remote from each other, from the working face of the probe and from the patient to achieve the required isolations. This invention overcomes these isolation problems while
25 achieving the needed high resolution of measurement.

BRIEF SUMMARY OF THE INVENTION

30 The present invention concerns a hybrid probe for both electrical and optical measurements in which the optical pathway and the optical sensors comprise elements located within a hybrid chip structure that is compact.

35 This invention overcomes the problems inherent in earlier designs of probes by siting the opto-electronics components in a high density array at the working face of the probe.

This is achieved by employing bare opto-electronic dice rather than packaged components and mounting these in close proximity to each other in an optimally designed chamber. Appropriate
5 electrical connections are made to these dice which are powered from electronics in the handle of the probe.

According to one aspect of the present invention there is disclosed an apparatus for
10 identifying different tissue types including those displaying modifications involving pre-cancerous or cancerous activity, said apparatus comprising a probe having one end shaped to face said tissue and having at least one radiation
15 source towards the end of the probe and a detector for that radiation and a comparator to compare the measured received radiation with known values to thereby identify the tissue type.

20 The apparatus may also include at least one electrode to apply electrical signals to the tissue and electrical means to measure the resulting electrical response by said tissue. A comparator is employed to compare the electrical and optical signals with a catalogue of
25 known tissue type signals to identify the tissue.

One difficulty with such a configuration is the need to isolate light emitting and light
30 receiving elements from one another. The hybrid probe is designed to examine areas of tissue having a diameter of the order of 2 mm, which requires that photodiode detectors be placed in close juxtaposition with light
35 emitters yet optically isolated so that light signals do not pass directly from an emitter to a detector without intervention (i.e., back-

scattering) by the tissue under examination. This is accomplished in the present invention by the use of metal barriers. The metal barriers also shield the detector circuitry from electrical interference carried by current pulses that must be applied to the LEDs to induce them to emit light. The metal barrier may be left floating or grounded, but can also serve an additional role as an electrode for making electrical measurements to replace or supplement the two or three noble metal electrodes adjacent to the hybrid circuit normally used for the electrical measurements to be made on the tissue.

15 In addition the hybrid structure provides a preamplifier in close proximity to the photodiodes to amplify the small current from the photodiode detectors and feed it to the electronics in the handle of the probe and from there to the analysis circuitry.

20 It has been pointed out above that the fiber-based probe is temperature sensitive. This temperature sensitivity often occurs at bends in the fiber. It is often not practical to measure these temperatures so compensation is difficult to achieve. A change in temperature at the tip of the probe is likely to occur when the probe is brought into contact with the tissue of a warm blooded being. The subject of this invention overcomes the forms of temperature sensitivity arising from the fibers. The radiation output of LEDs is also temperature sensitive but for precise measurements can be compensated by using a characteristic of the LED to determine its own temperature. The bandgap potential of LEDs is a known function of temperature, allowing the temperature to be

determined by applying a known current to the diode and measuring the potential across it. This can then be used to correct for the output of the LED using established equations thereby compensating for the changed radiation emission caused by temperature changes.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is an illustration of the layout of the tip of the probe as seen in perspective showing only optical components.

Figure 2 is an illustration of another embodiment that includes electrodes in the probe tip.

Figure 3 is an illustration in section of another embodiment of the invention having a multilayered substrate running along at least a portion of the length of the probe.

Figure 4 is an end view of the multilayered substrate embodiment from the probe tip end.

Figure 5 is a perspective view of the multilayered substrate embodiment.

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

To delineate the dimensions of a suspected area of abnormal tissue by the use of optical measurements to identify tissue types it is essential that the detector be able to resolve areas at a high resolution. The effective area that is illuminated by the radiation during the optical measurements therefore needs to be as small as possible, down to as little as one square millimeter. Below this dimension abnormalities are unlikely to affect the health of the patient since they will most likely spontaneously clear within a relatively short time.

To attain dimensions of this order it is necessary to crowd the opto-electronics into an extremely small volume. This places demands on the technology that is employed which were
5 heretofore unachievable. It is a feature of this invention that we have accomplished packing densities that have not been achieved previously. The invention also provides effective devices where three or more electrodes are
10 sited within the small dimensions of the assembly enabling electrical measurements to be made on essentially the same area of tissue as that measured optically. The invention provides a novel design layout solving these problems.

15 The layout described achieves the needed isolation of the input and output optical signals and the corresponding emitter driving currents from minuscule detector currents. This isolation is a critical requirement since
20 the optical losses involved in this method of measurement are great and effective shielding is vital. The opportunity for signal leakage is ever present since the drive currents to the LEDs are many orders of magnitude greater than
25 the detector currents. Isolation of the electrical measurements from the optical ones is conveniently achieved by performing the measurements sequentially but nearly simultaneously rather than precisely simultaneously.

30 The invention does not reside entirely in any particular layout. Other layouts of the components are feasible if the principles embodied in this invention are adhered to. These principles concern the isolation of elements and the maintaining of active elements in
35 close, but suitably spaced proximity to the tissue under examination. These principles are

described in part by the ends to be accomplished by suitable layouts and guidance is further given by specifying preferred layouts. For example the barrier can be used as an electrode for the purposes of tissue electrical measurements. By this means the electrical measurement can be placed in the center of the region of optical measurement, a desirable but not an essential feature.

Figure 1 shows a perspective view of the probe tip with the placement of the opto-electronic components clearly shown. This probe is useful to detect the onset of precancer or cancer within the endocervical canal or is in addition to making measurements on the outer parts of the cervix. As shown the hybrid probe has a cylindrical shape with a diameter of about 3 mm. The radiation sources 1 in this case are LEDs and three are shown in this assembly, located within a space 5 at the tip of the probe. They are mounted on a substrate 9 along with the other components. To control the direction of the radiation and to act as an electrostatic shield the barrier 2 divides the assembly into two chambers. This barrier must be electrically conductive to provide the needed electrical shielding. It can be grounded or left floating. In the far side chamber is located the radiation detector 3.

Figure 2 illustrates an embodiment of the invention that includes electrodes. In this embodiment electrodes 4 have been included in the assembly to enable electrical measurements to be made. Three are shown but the number can vary depending on other factors. The electrodes illustrated are circular but they may be of other dimensions. For example kidney-shaped

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electrodes offer advantages since they can be of greater area than by limiting the shape to circular. An advantage in adopting the kidney shape is to achieve the maximum possible electrode area without compromising the optical performance or the electrical resolution.

5 Larger electrodes by their nature produce less noisy data because they are sampling a larger area of tissue which is naturally less variable than a smaller area. The space 5 is typically filled with a transparent resin to hold the components in position and to protect them from damage. The assembly is mounted in a tube 6 which forms part of the completed probe. An

10 amplifier 7 boosts the signal from the detector 3 so that it can be conveyed back to the controller. The amplifier is mounted on a circuit board 8 which holds other circuits involved in driving the LEDs and electrodes. A critical

15 feature of this arrangement arises from the need to take special care with the shielding of the wiring from the detector 3 to its amplifier 7. The currents flowing in this wire may be of the order of nanoamperes. The drive current to

20 the nearby LEDs may be as high as 100 milliamperes. The ratio of these currents is huge so shielding is vital. In addition the patient's body may have substantial voltage signals present because of adjacent wiring or

25 other electrical equipment being operated nearby. The detector circuit must therefore be shielded from this source of interference as well. This is achieved by the use, for example, of multilayer circuit boards 8 to

30 convey the signals. The disposition of the signals flowing in the tracks on these boards must be chosen carefully to avoid unwanted

35

capacitive or electromagnetic coupling.

The optical layout needs to be planned because of the conflicting demands made on it. The radiation signal reaching the tissue needs to reach a level sufficient to compete with the ambient light level being employed for the operator's visual needs. LEDs have limited light output so as much as possible of this output radiation needs to be available to illuminate the tissue. To achieve this the LEDs 1 are placed as close as possible to the tissue. If, in fact, the efficiency of LEDs continues to improve, the above consideration may become less of a problem in the future.

There are two limits to how small the distance from the top of the LEDs to the tissue can be made. The first of these is the need to accommodate the bond wires 17 from the top of the LEDs which tends to loop upward from the surface of the LED die. The second arises from optical considerations. It is important to control the direction and angle of the illumination of the tissue surface so that probes behave consistently. If the distance between the opto-electronics and the tissue varies, the sensitivity of the device will vary. Tissue recognition will thereby be impaired. The distance from the LEDs to the tissue surface should therefore be kept large enough that assembly tolerances do not lead to uncontrolled variability between probes. Since the position and size of the LED top surface can typically be controlled to within plus or minus 25 micrometers, this uncertainty should not be more than, say, 5% of the LED to surface distance. That distance should therefore be not less than 0.5 millimeter.

The lateral placement of the dice is similarly controllable to only 25 micrometers so this needs to be factored in to the geometric considerations. More deeply placed dice
5 will be less sensitive to errors in placement.

The lateral placement also affects the diagnostic ability of the device by modifying the depth of penetration of the radiation prior to its return to the detector. It is important
10 therefore that the placement be chosen to achieve the desired depth of penetration bearing in mind the tolerances on the accuracy that can be maintained. In general the closer the opto-electronics components 1 and 3 are to the
15 barrier 2 the smaller the depth of penetration.

Figure 3 shows another embodiment of the invention. In this embodiment the optoelectronics components 1 and 3 are mounted on opposite sides of a multilayer PCB 11. The light
20 emitters 1 are on one side while the detector 3 is on the other. The detector is connected to the amplifier 7 which is mounted back from the tip.

Electrodes 13, 14 and 15 are situated
25 around the opto-electronics and electrodes 13 and 14 perform the additional duty of acting as radiation reflectors respectively to direct the radiation to the tissue and thence back to the detector after it has been backscattered.
30 Figure 4 shows an end view of the same embodiment.

Figure 5 shows a perspective view of the same embodiment. The controller, which is not illustrated, and may be remote from the probe
35 tip, connected by appropriate wiring, drives the radiation sources and measures the signals from the detector and from the electrodes when

they are included. It also applies a small current to the LEDs and measures the voltage drop to determine the temperature of the LEDs. It then calculates a correction for the radiation output from the LEDs and adjusts the measured values of the detector signal accordingly.

It is also possible to build the hybrid assembly into other forms such as a capsule with an extended lead. This enables the capsule to pass into internal organs such as the stomach or lungs. It could even be passed down thicker veins or arteries. An endoscopic type of mounting could be provided for the device.

The controller performs manipulations on the corrected signals from the probe and arrives at a decision as to the tissue type by comparing the data with a catalogue of data of known tissue types. The decision is then communicated to the operator via one of several means such as by means of colored lights on the probe, by an audible tone, or by a display on the controller.

Although the invention has been described in terms of preferred embodiments, it is intended that the protection afforded by this patent not be so limited, but be determined by the full valid extent of the following claims.

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What is claimed is:

1. Apparatus for identifying tissue which is suspected of being physiologically changed, said apparatus comprising:

5 a probe having a tip comprising a close packed array of components, said components comprising

10 at least one emitter, each emitter comprising a light emitting die, said light emitting die configured to irradiate said tissue;

15 at least one detector, each detector comprising a detector die, said detector die configured to receive that radiation after it has been backscattered by said tissue;

20 a shield comprising an electrode for making electrical measurements on said tissue and sited between said at least one emitter and said at least one detector to prevent leakage of optical and electrical signals from one to the other;

25 said apparatus further comprising a controller coupled to the at least one emitter and the at least one detector that supplies drive signals and receives responses, said controller comprising

a processor for said responses in combination in order to categorize said tissue, and

30 a comparator for comparing the categorization of said tissue with expected tissue types from a catalogue so as to identify said tissue, and

35 an indicator arrangement for indicating to a user the tissue type identified.

2. The apparatus for identifying tissue of claim 1 wherein said electrode is configured to supply electrical signals to said tissue and to receive electrical responses from the tissue.

5 3. The apparatus for identifying tissue of claim 1 further comprising an amplifier in close proximity to said at least one detector.

10 4. Apparatus as claimed in any one of claims 1, 2, or 3 further comprising
a circuit that feeds current to a light emitting die in the probe tip
said at least one detector having wiring that is shielded electrically by a conductive metal surface mounted in close proximity to the
15 wiring, wherein said surface reduces the capacitive coupling of the wiring to said circuit and wherein said surface further reduces the capacitive coupling to a patient during an examination with the apparatus thereby reducing
20 the amount of cross coupling and electrical interference.

5. An apparatus as claimed in one of claims 1, 2, 3, or 4, in which
each emitter comprises
25 an LED that receives a current and outputs radiation in response to the current and the apparatus further comprises
means to adjust signals received from the at least one detector, said means to adjust
30 comprising
means to measure a voltage drop to determine the temperature of the LED and
means to calculate from said measured voltage drop a correction for the radiation

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output from the LED.

6. Apparatus for identifying tissue which is suspected of being physiologically changed, said apparatus comprising:

5 a probe having a tip comprising a close packed array of components, said components comprising

a light emitting die configured to irradiate said tissue;

10 a detector die configured to receive radiation backscattered by said tissue;

a shield sited between said light emitting die and said detector die to prevent leakage of optical and electrical signals from one to the other;

15 an electrode configured to supply electrical signals to said tissue and to receive an electrical response from the tissue;

said apparatus further comprising
20 a controller coupled to said emitter die, said detector die and said electrode that supplies drive signals and receives the responses, said controller comprising

a processor for said responses in
25 combination in order to categorize said tissue, and

a comparator for comparing the categorization of said tissue with expected tissue types from a catalogue to identify said
30 tissue, and

an indicator arrangement for indicating to a user the tissue type identified.

7. Apparatus for identifying tissue of claim
35 6 wherein said probe tip comprises a capsule

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with an extended lead to enable said capsule to pass into internal organs.

5 8. Apparatus for identifying tissue which is suspected of being physiologically changed as a result of pre-cancerous or cancerous activity, said apparatus comprising:

a probe having a tip comprising a close packed array of components, said components comprising

10 at least one emitter comprising a light emitting die, said light emitting die configured to irradiate said tissue;

15 at least one detector comprising a detector die, said detector die configured to receive that radiation after it has been backscattered by said tissue;

20 a shield sited between said at least one emitter and said at least one detector to prevent leakage of optical and electrical signals from one to the other;

said apparatus further comprising

25 a controller coupled to said at least one emitter and said at least one detector that supplies drive signals and receives responses, said controller comprising

a processor for responses in combination in order to categorize said tissue, and

30 a comparator for comparing the categorization of said tissue with expected tissue types from a catalogue so as to identify said tissue, and

an indicator for indicating to a user the tissue type identified,

35 a circuit that feeds current to the light emitter in the probe tip

said at least one detector having wiring that is shielded electrically by a conductive metal surface mounted in close proximity to the wiring, wherein said surface reduces the capacitive coupling of the wiring to said circuit and wherein said surface further reduces the capacitive coupling to a patient during an examination with the apparatus thereby reducing the amount of cross coupling and electrical interference.

9. An apparatus as claimed in one of claims 6, or 8, wherein said electrode is a kidney-shaped electrode in the probe tip .

10. Apparatus as claimed in any one of claims 6 or 8, further comprising
a circuit that feeds current to the light emitting die in the probe tip

said detector die having wiring that is shielded electrically by a conductive metal surface mounted in close proximity to the wiring, wherein said surface reduces the capacitive coupling of the wiring to said circuit and wherein said surface further reduces the capacitive coupling to a patient during an examination with the apparatus thereby reducing the amount of cross coupling and electrical interference.

11. An apparatus as claimed in one of claims 6 or 8, in which

said light emitting die comprises
an LED that receives a current and output radiation in response to the current and the apparatus further comprises
means to adjust signals received from the

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detector die, said means to adjust comprising
means to measure a voltage drop to
determine the temperature of the LED and
means to calculate from said measured
5 voltage drop a correction for the radiation
output from the LED.

12. Apparatus for identifying tissue which is
suspected of being physiologically changed said
apparatus comprising:

10 a probe having a tip comprising a close
packed array of components, said components
comprising

at least one LED that receives a
current and outputs radiation in response to
15 the current to irradiate said tissue;

at least one detector configured to
receive that radiation after it has been
backscattered by said tissue and to provide
signals;

20 a shield sited between said at least
one LED and said at least one detector to
prevent leakage of radiation and electrical
signals from one to the other;

said apparatus further comprising
25 means to adjust signals provided by the
detectors, said means to adjust comprising
means to measure a voltage drop to
determine the temperature of the at least one
LED, and

30 means to calculate a correction for
radiation output from the at least one LED,
a controller coupled to said at least one
LED and detector, said controller comprising
a processor for said responses in
35 combination in order to categorize said tissue,
a comparator for comparing the

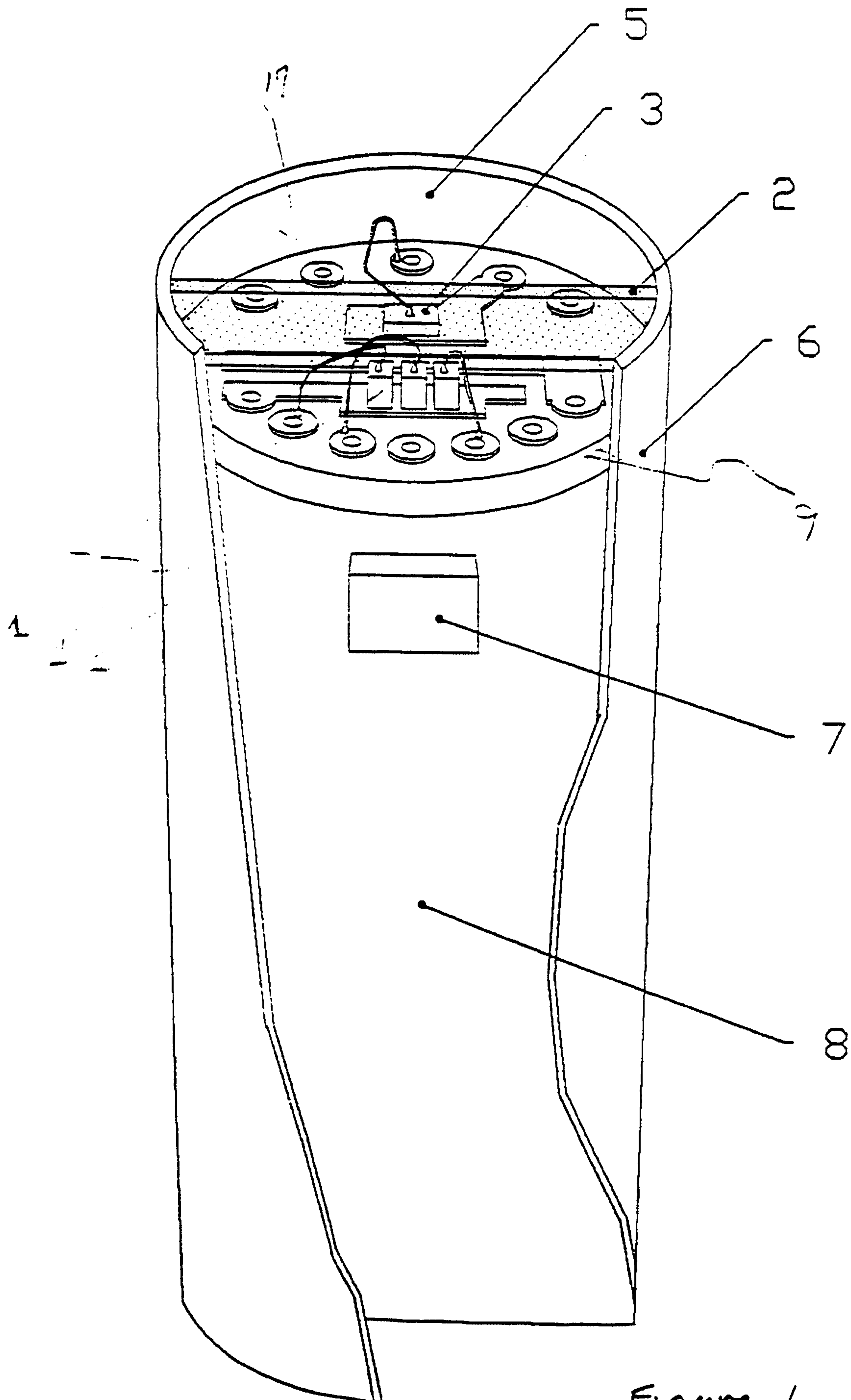
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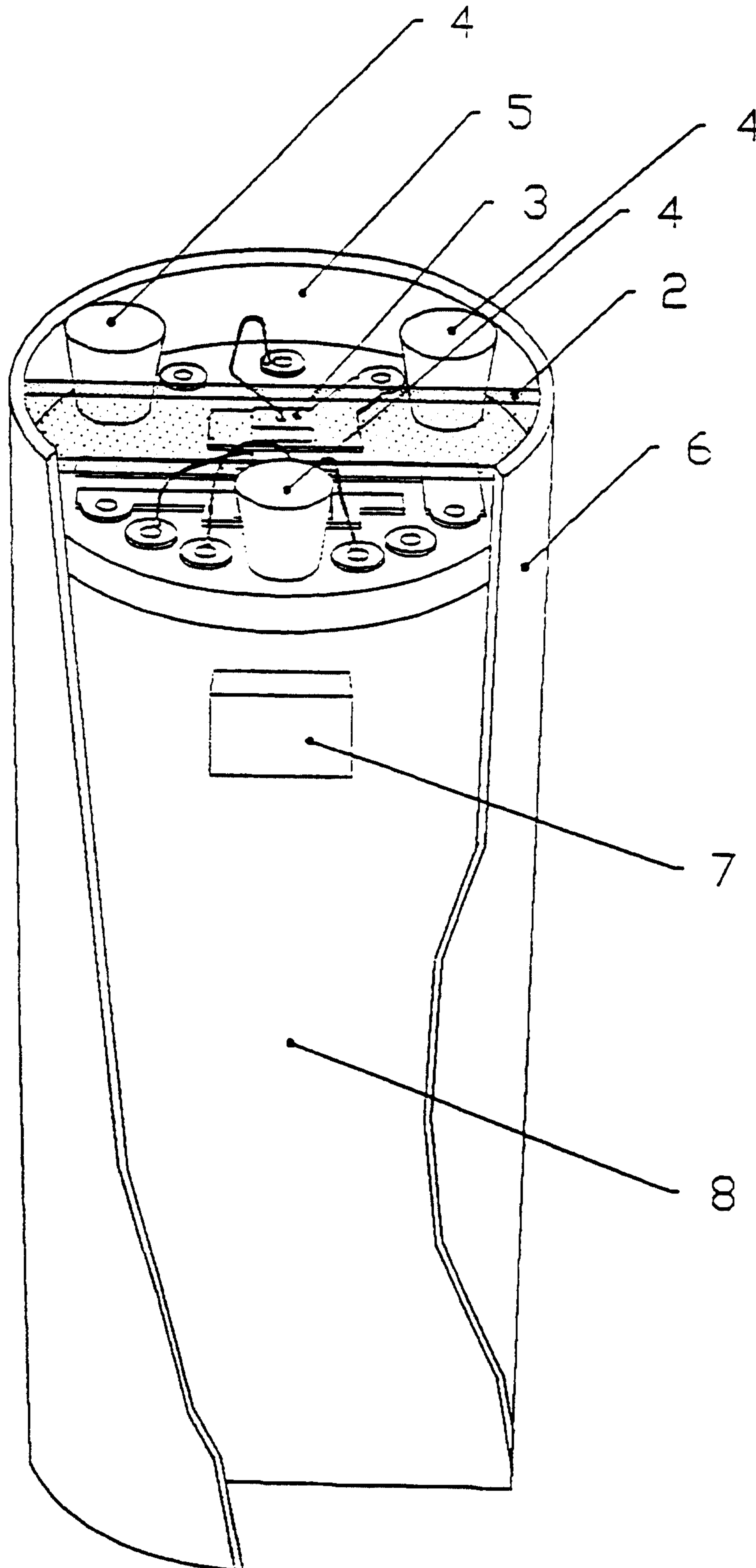
categorization of said tissue with expected tissue types from a catalogue so as to identify said tissue, and

5 an indicator arrangement for indicating to a user the tissue type identified.

13. The apparatus for identifying tissue of claim 10 further comprising an amplifier in close proximity to said at least one detector.

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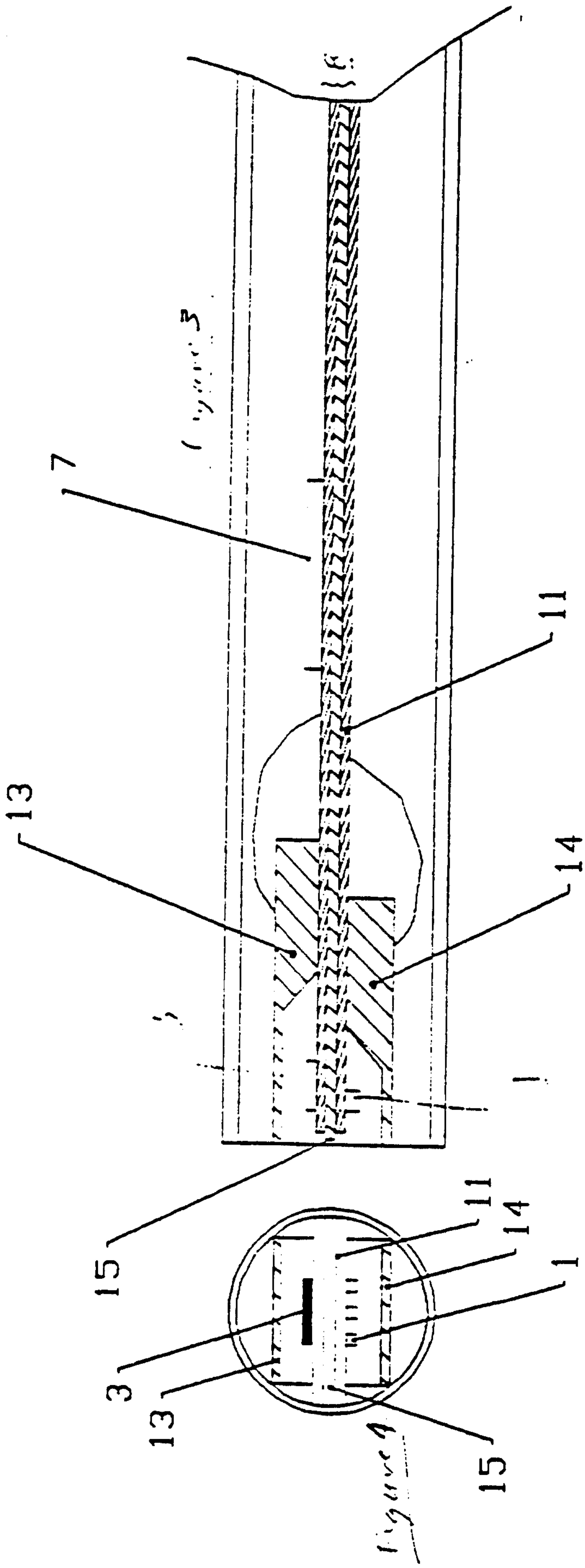
Figure 1



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Figure 2

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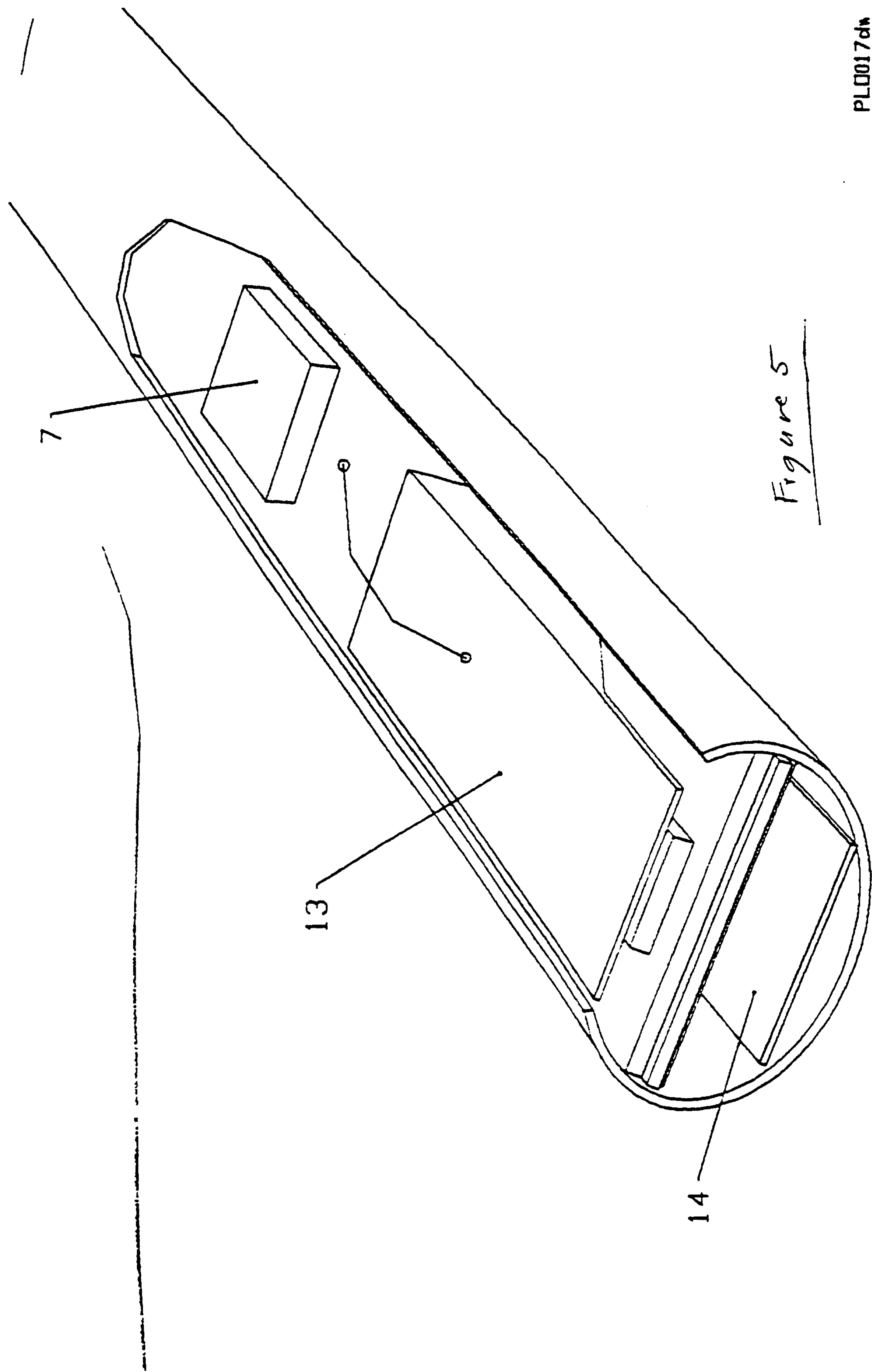


Figure 5