



(86) Date de dépôt PCT/PCT Filing Date: 2001/04/10

(87) Date publication PCT/PCT Publication Date: 2002/11/14

(45) Date de délivrance/Issue Date: 2008/08/05

(85) Entrée phase nationale/National Entry: 2002/11/14

(86) N° demande PCT/PCT Application No.: DE 2001/001398

(87) N° publication PCT/PCT Publication No.: 2001/080919

(30) Priorités/Priorities: 2000/04/11 (US60/196,083);
2000/04/22 (DE100 19 982.8)

(51) Cl.Int./Int.Cl. *A61L 27/34* (2006.01),
A61L 29/08 (2006.01), *A61L 31/10* (2006.01),
A61L 33/06 (2006.01), *C08G 79/02* (2006.01),
C08J 5/18 (2006.01)

(72) Inventeurs/Inventors:
GRUNZE, MICHAEL, DE;
GRIES, CLAUDIA, DE

(73) Propriétaire/Owner:
CELONOVA BIOSCIENCES GERMANY GMBH, DE

(74) Agent: MOFFAT & CO.

(54) Titre : REVETEMENTS ET PELLICULES POUR INSTRUMENTS MEDICAUX A BASE DE POLY(TRIFLUORO-ETHOXYPHOSHAZENE)

(54) Title: POLY-TRI-FLUORO-ETHOXYPOLYPHOSHAZENE COVERINGS AND FILMS FOR MEDICAL DEVICES

(57) **Abrégé/Abstract:**

The present invention relates to an anti-thrombogenic, physically well-tolerated polymer and its use for manufacturing sheaths and films as a component of therapeutic devices for preventing excessive cell proliferation. Furthermore, it relates to films made from the polymer as well as wrappings for medical devices such as stents. It also relates to medical devices that are enclosed by a film or wrapping according to the invention.

Abstract

The present invention relates to an anti-thrombogenic, physically well-tolerated polymer and its use for manufacturing sheaths and films as a component of therapeutic devices for preventing excessive cell proliferation. Furthermore, it relates to films made from the polymer as well as wrappings for medical devices such as stents. It also relates to medical devices that are enclosed by a film or wrapping according to the invention.

Specification

The present invention relates to an anti-thrombogenic, physically well-tolerated polymer and its use for manufacturing sheaths and films as a component of therapeutic devices for preventing excessive cell proliferation. Furthermore, it relates to films made from the polymer, as well as wrappings for medical devices, such as stents. It also relates to medical devices that are enclosed by a film or wrapping according to the invention.

The biggest complications caused by artificial implants are the increasing platelet deposits on the exogenous surface. In addition, the behavior toward bacteria, macrophages and proteins deposited on the surfaces of the implant plays a central role, since these deposits contribute significantly to inflammation and other problems as the implant grows in.

One of the problems that can potentially occur is increased cell proliferation and inflammation of injured tissue that comes into contact with the artificial implant. In addition to the already known problems of increased thrombogenesis, restenosis (i.e., the re-constriction of blood vessels in an area dilated by angioplasty, often the stent area) is encountered in vascular implants, e.g., so-called stents. Among other things, these complications may stem from the activation of the coagulation and immune system by the implanted foreign body, and from damage done to the vascular wall while implanting the stent during an angioplasty. The result is so-called restenosis (re-occlusion of blood vessels), and possible inflammations in the treated area, which necessitate immediate drug therapy, and frequently surgical treatment as well.

25

One way in which an attempt is made to prevent these complications caused by an increased cell proliferation in the stent area, involves the use of sheathed, so-called *covered* stents. A wide range of materials and sheathed stents used for manufacturing such wrappings have become known and been investigated in prior art. For example, an expandable wrapping made from e-PTFE is used for this purpose in WO 9856312. Other

30

materials for this application are cited in EP 0810845, and, for example, mention polymers cited in US 4,883,699 and US 4,911,691. Other polymers named for the specified purpose include hydrolyzed polyacrylonitrile (US 4,480,642), hydrophilic polyethers (US 4,798,876) and polyurethane-di-acrylate (US 4,424,395). Also known are
5 different hydrogels that can be used for this purpose. The group of potentially applicable materials can also be supplemented with polyvinyl pyrrolidone (PVP) polymers, polyvinyl alcohols (PVA), p(polyethylene oxide) polymers (PEO) and poly hydroxyethyl methacrylate p(HEMA). Furthermore, publications mention the use of a group of standard materials like polyurethane, polyethylene and polypropylene as possible materials. Also
10 known are mixtures of these materials with each other. A group of additional materials is also known from EP 0804909.

The properties of these compounds are variable, and it may be assumed that each of these materials exhibits special properties for specific applications. For example, PVA is
15 readily soluble in liquids. Other materials have good blood tolerance. Still other materials are highly extensible. However, all materials unfortunately exhibit shortcomings in certain areas. PVA, for example, does not possess an especially good blood tolerance. ϵ -PTFE has very good extensibility, for example, and also good blood tolerance, but this material is extremely difficult to work with, and manufacturing such wrappings requires a
20 series of processing steps (WO 96/00103). With other materials, elastic properties can only be achieved by adding softeners, which lower tolerance in the blood and body, and also burden the patient owing to the elimination of the "softeners".

Among other things, this means that due to the inadequate properties of existing materials
25 during postoperative treatment after an angioplasty, patients must currently be given anticoagulants (vitamin K antagonists). Determining the dosages of the latter is problematical, however.

This also means that the restenosis rate lies at approx. 30-50% within 6 months of an
30 angioplasty for commercially available stents.

This rate should be lowered through the use of sheathed stents, by preventing cellular tissue from growing in the vascular space. However, this technology comes up against limiting factors determined above all by the materials, their physicochemical properties,
5 and the surface quality of these materials.

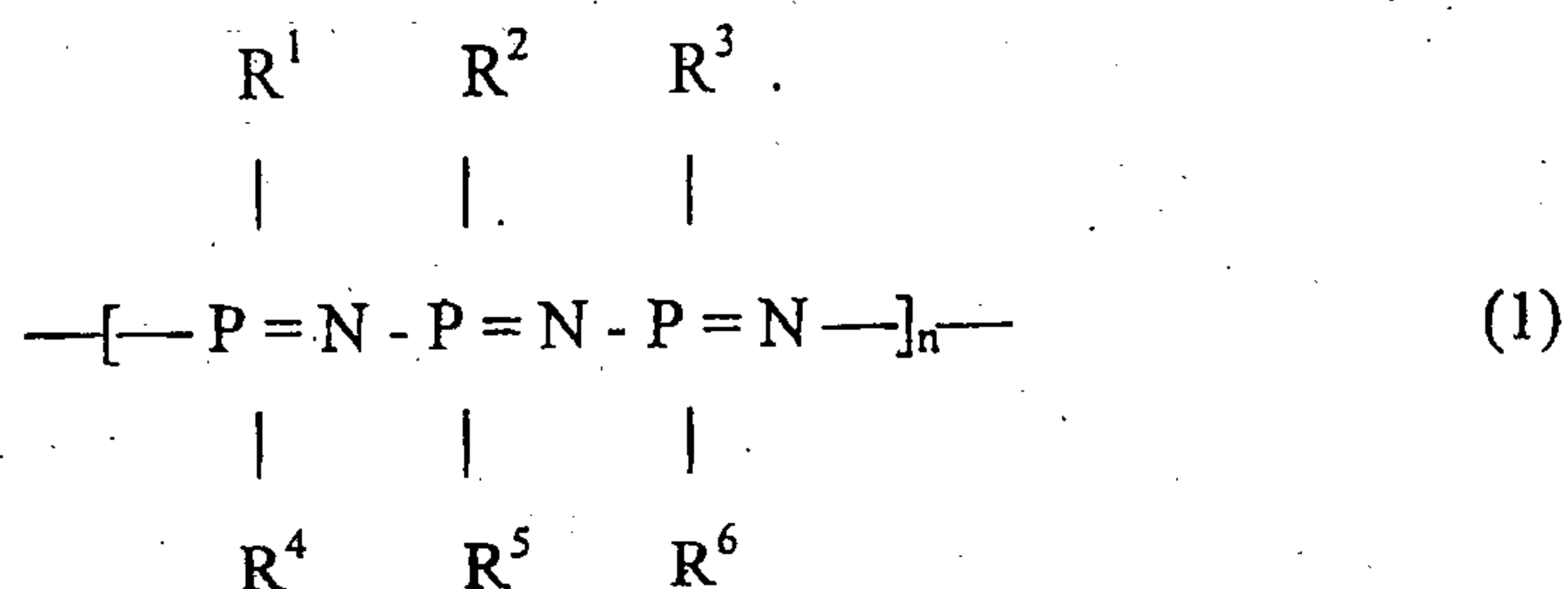
The polymeric compound poly [bis(trifluoroethoxy) phosphazene] exhibits a good antithrombogenic effect as a bulk material (cf. Tur, *Untersuchungen zur Thrombenresistenz von Poly[bis(trifluoroethoxy)phosphazen]* and Hollemann-Wiberg
10 "Stickstoffverbindungen des Phosphors" *Lehrbuch der anorganischen Chemie* 666-669, 91st -100th Edition, Walter de Gruyter Verlag 1985 also Tur, Vinogradova, et al., "Entwicklungstendenzen bei polymeranalogen Umsetzungen von Polyphosphazene," *Acta Polymerica* 39: 424-429, (8) 1988). Moreover, polyphosphazene was used in Patent Specification DE 196 13 048 as a coating for artificial implants.

15

However, this substance alone cannot limit or reduce the cell growth that leads to restenoses.

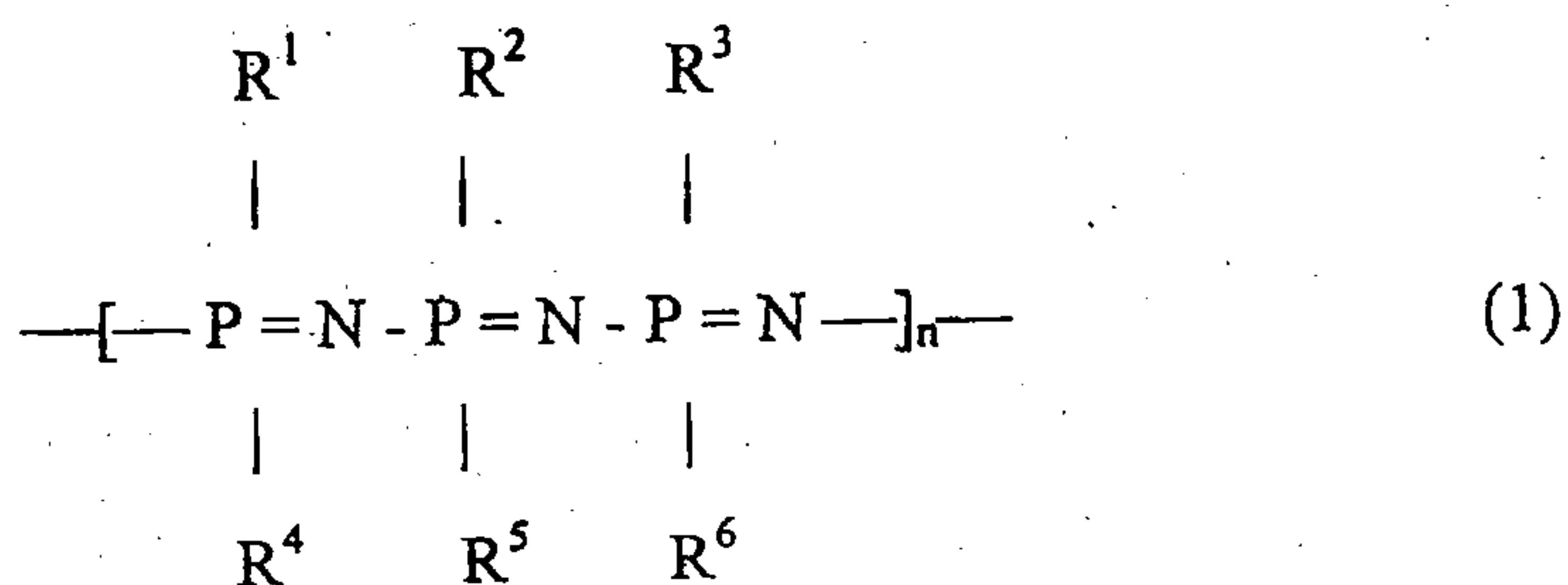
Therefore, the object of the present invention is to provide a film and a wrapping made
20 from it for medical devices, e.g., catheters or stents of all types, which on the one hand exhibit excellent mechanical and physical tolerance properties, so as to improve the biocompatibility of sheathed medical devices, while on the other hand preventing or diminishing the aforementioned secondary injuries following treatment or implantation. In particular, supplying the specified film and the device fabricated from it is for
25 preventing or diminishing uncontrolled cellular growth, e.g., which leads to restenoses after stent implantation. Additionally to be achieved is a decrease in inflammatory reactions, which are a common response to the introduction of a foreign material into the body, and require the administration of antibiotics.

This object is achieved by supplying a film for the sheathing of a medical device, wherein the film comprises a biocompatible polymer with the following general formula (1),



where n is 2 to ∞ , R¹ to R⁶ are either the same or different and each is selected from an alkoxy of from 1 to 20 carbon atoms, an alkylsulfonyl of from 1 to 20 carbon atoms, a
 5 dialkyl amino of from 1 to 20 carbon atoms, an aryloxy group, a heterocyclic alkyl with a nitrogen heteroatom and a heteroaryl group with a nitrogen heteroatom.

The present invention also provides a method of manufacturing a microstructured film for sheathing of a medical device, comprising the steps of: a) coating a microstructured stamp with a biocompatible polymer in a solvent, said biocompatible polymer having the
 10 following general formula:



where n is 2 to ∞ , R¹ to R⁶ are either the same or different and each is selected from an alkoxy of from 1 to 20 carbon atoms, an alkylsulfonyl of from 1 to 20 carbon atoms, a dialkyl amino of from 1 to 20 carbon atoms, an aryloxy group, a heterocyclic alkyl with a

nitrogen heteroatom and a heteroaryl group with a nitrogen heteroatom, b) evaporating the solvent, c) peeling the resultant film off the microstructured stamp.

5 The degree of polymerization of polymers according to formula (1) used to manufacture the film according to the invention and wrapping fabricated from it is to range from 2 to ∞ . However, the degree of polymerization preferably ranges from 20 to 200,000 and more preferably from 40 to 10,000,000.

Furthermore, the polymer used for manufacturing purposes is to satisfy the following requirements:

10 At least one of the groups R^1 to R^6 in the polymer is preferably an alkoxy group substituted with at least one fluorine atom.

The alkyl group in the alkoxy, alkylsulfonyl and dialkyl amino groups include straight or branched chain alkyl groups with 1 to 20 carbon atoms, wherein the alkyl groups may be substituted with at least one halogen atom, such as a fluorine atom.

Examples of alkoxy groups include methoxy, ethoxy, propoxy and butoxy groups, which preferably can be substituted with at least one fluorine atom. Particularly preferred is the 2,2,2-trifluoroethoxy group. Examples of alkylsulfonyl groups are methyl, ethyl, propyl and butylsulfonyl groups. Examples of dialkyl amino groups are the dimethyl, diethyl, 5 dipropyl, and dibutylamino groups.

The aryl group in the aryloxy group is, for example, a compound with one or more aromatic ring systems, wherein the aryl group can be substituted with at least one of the previously defined alkyl groups, for example. Examples of aryloxy groups are phenoxy 10 and naphthoxy groups and derivatives thereof.

The heterocyclic alkyl group is for example a 3 or 7 membered ring system wherein at least one ring atom is a nitrogen atom. The heterocyclic alkyl group can, for example, be substituted by at least one of the previously defined alkyl groups. Examples of 15 heterocyclic alkyl groups include piperidinyl, piperazinyl, pyrrolidinyl and morpholinyl groups and derivatives thereof. The heteroaryl group can be a compound with one or more aromatic ring systems, wherein at least one ring atom is a nitrogen atom. The heteroaryl group can be substituted with at least one of the previously defined alkyl groups, for example. Examples of heteroaryl groups include pyrrolyl, pyridinyl, 20 pyridinoyl, isoquinolinyl, and quinolinyl groups and derivatives thereof.

In a preferred embodiment of the present invention, the film according to the invention and the wrapping fabricated from it using the polymer, consist of poly[bis(trifluoroethoxy)phosphazene] marked with ^{32}P , ^{33}P , or As or Sb isotopes. 25

The present invention also relates to the use of the film according to the invention and the sheath fabricated from it for the manufacture of a therapeutic device enveloped with this film for preventing excessive cell proliferation. Moreover, the film according to the invention and the sheath fabricated from it can be a constituent of other therapeutic

devices, such as artificial implants, plaster or tape, artificial blood vessels, stents, catheters, ureters, or other implants without direct contact with the blood.

5 The film according to the invention and the sheath fabricated from it can be used in conjunction with a coating or without any special pretreatment of the implant. Further, not only can the sheathed stents according to the invention be used in arterial vessels, but also in venous vessels, in the gastrointestinal tract, in the esophagus or trachea, or the urinary tracts.

10 Further, the present invention supplies a therapeutic device having a sheath made out of the polymer according to formula (1).

In a preferred embodiment of the present invention, an artificial implant material is supplied, which comprises an implant material as substrate and a biocompatible coating
15 that consists of the polymer with the aforementioned general formula (1) and is applied at least partially on the substrate surface.

The biocompatible coating of the artificial implant according to the invention has, for example, a thickness of about 1 nm to about 100 μm , preferably up to about 10 μm , and
20 especially preferred up to about 1 μm .

The implant material used as the substrate according to the invention has no special limitation, and can be any implant material, such as plastics, metals, metal alloys and ceramics. In particular, the implant material can be a ceramic or a metallic stent material.
25

In another embodiment of the artificial implant according to the invention, a layer containing an adhesion promoter is incorporated between the surface of the substrate and the biocompatible coating consisting of the polyphosphazene derivative.

The adhesion promoter or spacer preferably contains a polar end-group. Examples include hydroxy, carboxy, carboxyl, amino, or nitro groups. However, use can also be made of type O - ED end groups, wherein O - ED stands for an alkoxy, alkylsulfonyl, dialkyl amino, or aryloxy group, or a heterocycloalkyl or heteroaryl group with nitrogen as the heteroatom, and can be varyingly substituted, e.g., by halogen atoms, especially fluorine.

In particular, the adhesion promoter can be an organosilicon compound, preferably an amino-terminated silane, or based on aminosilane, amino-terminated alkenes, nitro-terminated alkenes, and silanes, or an alkylphosphonic acid. Aminopropyl trimethoxy silane is especially preferred.

In particular, the adhesion promoter improves adhesion of the coating to the surface of the device or implant material by coupling the adhesion promoter to the surface of the implant material, e.g., via ionic and/or covalent bonds, and by further coupling the adhesion promoter to reactive components, especially to described general formula (1) polymers of the coating, for example via ionic and/or covalent bonds.

In general, the film according to the invention and the wrapping are manufactured as follows:

20

A solution containing at least one compound with general formula (1) in a concentration of 0.1 % to 99 %, in a solvent, wherein this solvent is organic and polar. For example, ethyl acetate, acetone, THF, toluene, or xylenes can be used here. Mixtures of these solvents can also be used, or supplemented with other solvents. This solution is applied to a substrate that exhibits little or no adhesion to the polymer, e.g., glass, silicon, various ceramics or other appropriate materials, like polymers (PDMS, Teflon, PMMA, polycarbonate or silicones). The surfaces of the specified substrates surfaces can also be chemically modified, e.g., by introducing specific functional groups (-NH₂, -OH, -COOH, -COH, -COOMe, -CF₃, etc.).

30

Although the solvent can be evaporated without any additional measures, the solvent vapor concentration over the substrate is optimally set in a controlled manner, as is also the pressure and the temperature. At the start of the initial drying phase, the atmosphere over the coated substrate is to be saturated with solvent vapor, and the solvent vapor
5 concentration is then slowly reduced over a period of several hours. The temperature can vary from -30°C up to $+90^{\circ}\text{C}$. The pressure during the initial drying phase can range from normal pressure to water jet pressure (20 Torr). After the initial drying phase, the coated substrate is dried further for a fixed time in an oil-pump vacuum (0.1 Torr).

10 The polymer of compound 1 dried on the substrate can then be peeled off the substrate as a film. Depending on the concentration of the polymer solution of compound 1 and the particular conditions during the first drying phase, this yields films of varying layer thickness ranging from $0.1\text{ }\mu\text{m}$ to $300\text{ }\mu\text{m}$ or more, preferably ranging from $0.5\text{ }\mu\text{m}$ to $30\text{ }\mu\text{m}$, and especially preferred measuring around $5\text{ }\mu\text{m}$.

15

In a particular embodiment, the films or wrapping can also be microstructured according to the specified steps.

In this case, the substrate onto which the solution of compound (1) is applied is

20 microstructured. The structure of the substrate is carried over 1:1 to the structure of the film of the used polymer. One is not limited by the structural size of the substrate.

Therefore, structures on the order of nanometers, microns or even larger or smaller can be manufactured. In addition, the embodiment used in structuring is subject to no limitation.

This makes it possible to manufacture and use all structures that can be generated via

25 photolithography, electron beams or ion beams, or lasers or other techniques. In particular, structures having an especially favorable flow profile can be generated. These include lotus structures or structures resembling the "shark skin" known from aircraft construction. The special advantage to these structures and their use in manufacturing films and wrappings lies in the reduction of so-called contact activation of the
30 coagulation system.

The polymer of compound 1 dried on the substrate can then be peeled off the substrate as a structured film and further processed. Depending on the concentration of the polymer solution of compound 1 and the discussed conditions during the first drying phase, this
5 yields films of varying layer thickness ranging from 0.1 μm to 300 μm or more, preferably ranging from 0.5 μm to 30 μm , and especially preferred measuring around 5 μm .

The film microstructure can also be obtained by directly "writing" on the already present
10 film itself by means of laser, electron, or X-rays, or through "melt structuring", wherein a thin wire is brought to the melting point of the polymer, and then melts the desired structure into the film via direct contact.

Special advantages can be achieved by means of this structuring by impressing structures
15 in the film that impart a particularly favorable flow behavior to liquids (e.g., shark skin or lotus effect). This makes it possible to further diminish the contact activation of blood and further ameliorate the risk of thrombocyte aggregation in the case of sheathed stents. However, this type of structuring is not limited to the manufacture of sheathed stents, but can also be used to fabricate catheters or tubing in continuous flow systems, such as
20 support systems, angioplasty catheters, ureters, etc. Similarly, the inner parts of dialysis devices can be shaped in this way, for example, thereby reducing the need for Heparin.

The wrapping is manufactured according to the following procedure.

25 The film of compound 1 obtained according to the above process is tailored to the size of the stents (+2 mm). The stents are then placed in a mount and wound with the film of compound 1 in such a way that the film extends a uniform 1 mm over both ends. The film wound around the stents can be one or more layers thick. The ends of the wrapping produced in this way along with the individual layers of the film are then heat-sealed on
30 all sides, inside and outside, "welded" in the hot solvent vapor. To this end, the solvent is

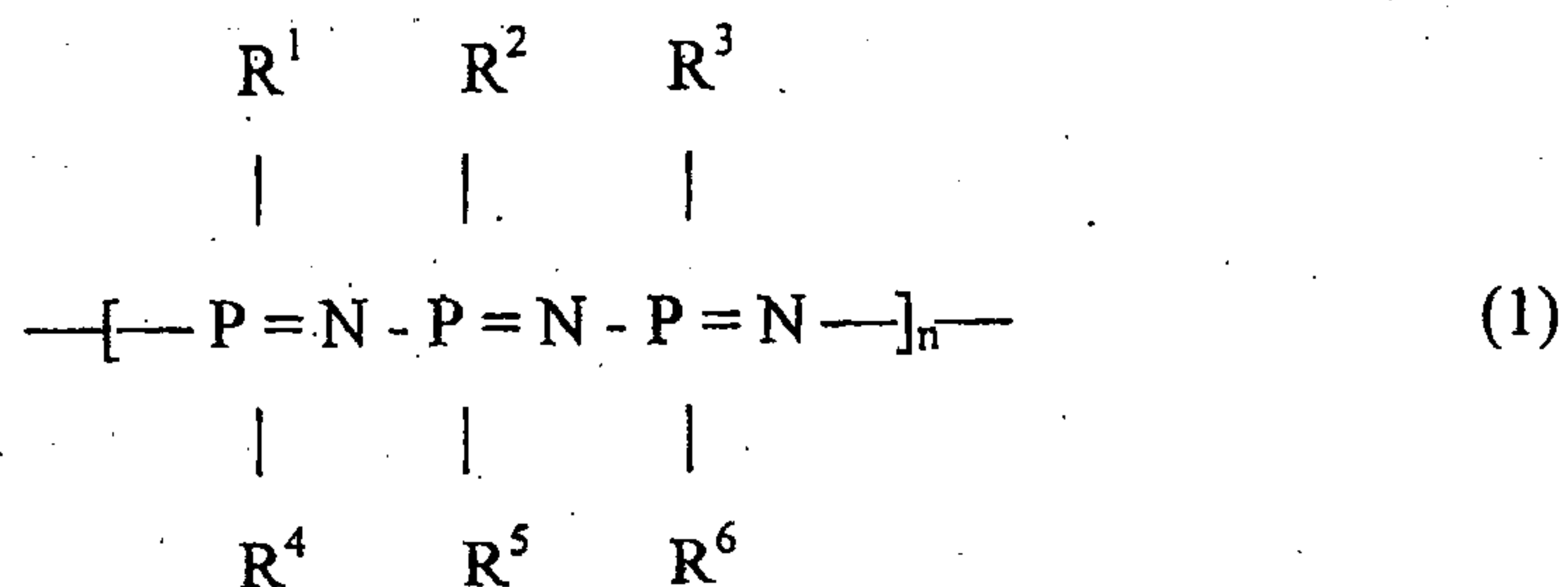
heated to a temperature of 40-120°C, optimally to 80°C or a higher temperature. The solvent vapor rises and flows out of a very fine tube provided with one or more nozzles. Depending on its length and material, this tube can be heated and is held at a specific angle to the rising solvent vapor, so that the solvent vapor that partially condenses in the
5 nozzle tube can drain back into the vessel without jamming the nozzles or impeding the outflow of rising solvent vapor.

The implants also obtained using the film and sheathing according to the invention surprisingly retain the excellent mechanical properties of the device and implant material.
10 This not only improves the biocompatibility of such artificial implants, but also reduces uncontrolled cell growth, which, for example, leads to restenoses after a stent implant, by preventing cell growth in the vascular space. Moreover, using a microstructured film according to the invention makes it possible to virtually forestall the contact activation of the coagulation system.

15

WE CLAIM:

1. A film for the sheathing of a medical device, wherein the film comprises a biocompatible polymer with the following general formula (1),



where n is 2 to ∞ , R^1 to R^6 are either the same or different and each is selected from an alkoxy of from 1 to 20 carbon atoms, an alkylsulfonyl of from 1 to 20 carbon atoms, a dialkyl amino of from 1 to 20 carbon atoms, an aryloxy group, a heterocyclic alkyl with a nitrogen heteroatom and a heteroaryl group with a nitrogen heteroatom.

2. The film for sheathing of a medical device according to claim 1, wherein the film is a film for sheathing a medical device which is selected from an artificial implant, a plaster, an artificial blood vessel, a stent, a catheter, a ureter and an implant which does not directly contact blood.

3. The film according to claim 1 or 2, wherein the film is a microstructured film.

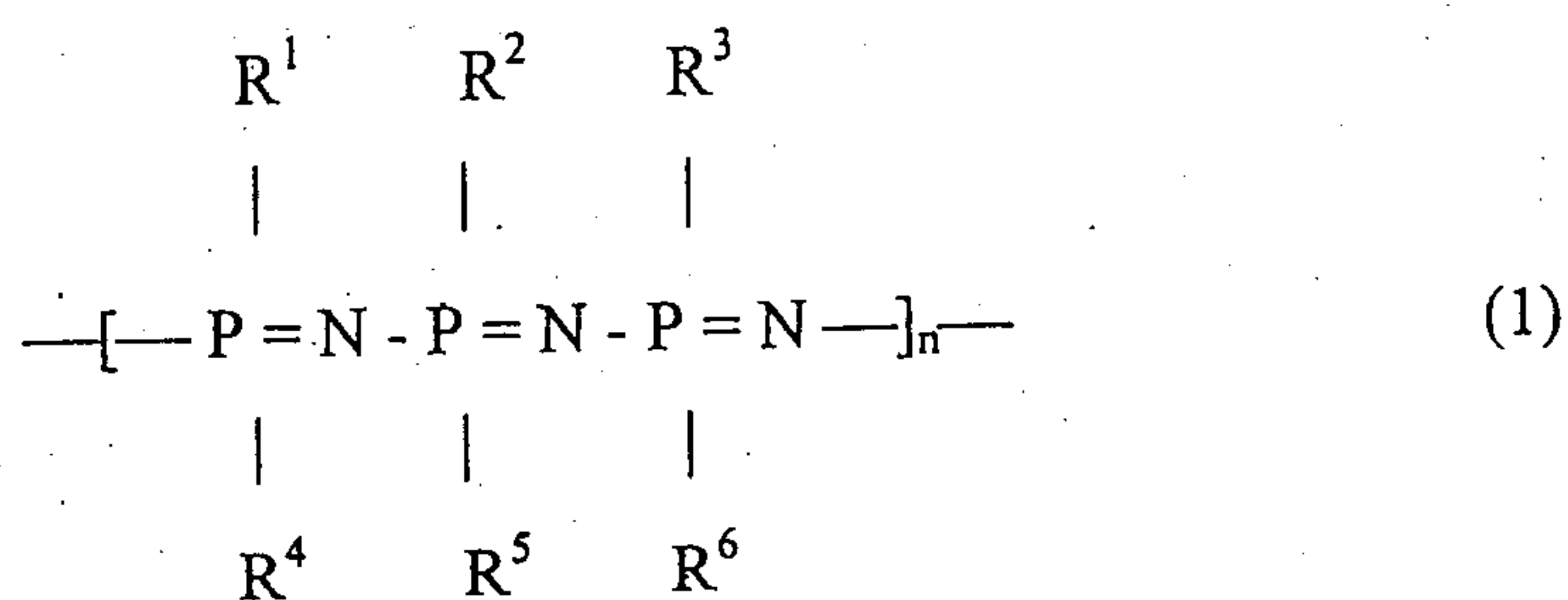
4. The film according to claim 3, wherein structures of the microstructured film are uniform.

5. The film according to claim 4, wherein a surface of the microstructured film has structures which provide flow properties that diminish the contact activation of blood.

6. The film according to claim 1 or 2, wherein the film is a microstructured film, in which a structure is generated directly by means of laser, electron, x-rays, or a heated wire on the film.

7. A method of manufacturing a microstructured film for sheathing of a medical device, comprising the steps of:

a) coating a microstructured stamp with a biocompatible polymer in a solvent, said biocompatible polymer having the following general formula:



where n is 2 to ∞ , R^1 to R^6 are either the same or different and each is selected from an alkoxy of from 1 to 20 carbon atoms, an alkylsulfonyl of from 1 to 20 carbon atoms, a dialkyl amino of from 1 to 20 carbon atoms, an aryloxy group, a heterocyclic alkyl with a nitrogen heteroatom and a heteroaryl group with a nitrogen heteroatom,

b) evaporating the solvent,

c) peeling the resultant film off the microstructured stamp.

8. A method as claimed in claim 6, wherein said stamp has uniformly distributed microstructures on the surface thereof.

9. A method as claimed in claim 7, wherein said solvent is a polar solvent.